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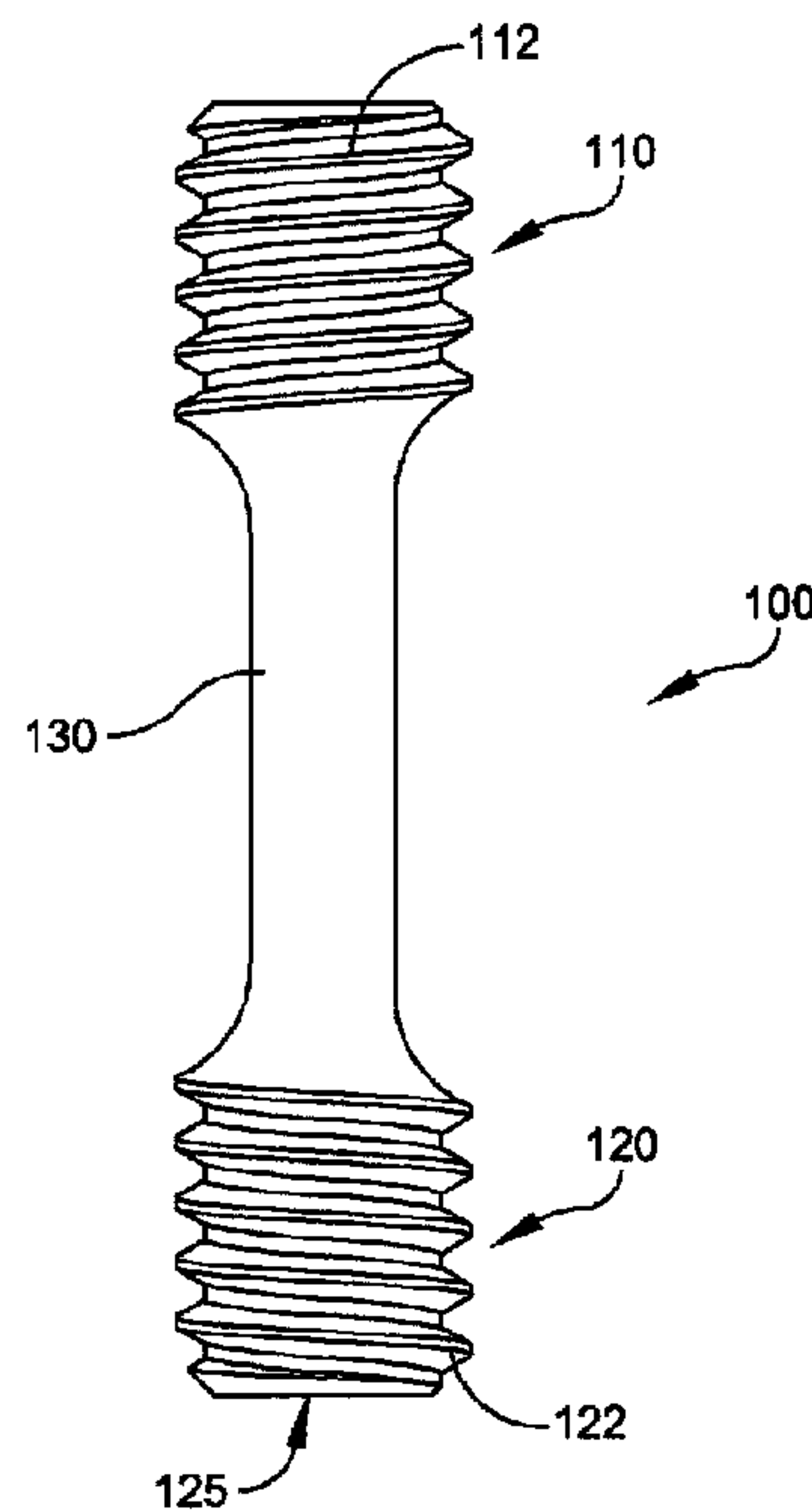
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(54) **Titre : DISPOSITIF DE COMPRESSION D'ORTEIL EN MARTEAU A FILET DOUBLE**

(54) **Title: DOUBLE THREAD HAMMERTOES COMPRESSION DEVICE**



(57) **Abrégé/Abstract:**

A method and device to correct hammertoes. The device includes an elongated device having a first threaded end with a first thread pitch and a second threaded end with a second thread pitch. A core connects the first and second threaded ends. When the implant is implanted into a joint and rotated about its longitudinal axis when mated with a driver, a target joint may be compressed using the first thread pitch on a distal bone in the joint and the second thread pitch on a proximate bone in the joint. The first and second thread pitches may be the same but in opposing directions, may be different but in the same direction, or may be different and in opposing directions.

ABSTRACT

A method and device to correct hammertoes. The device includes an elongated device having a first threaded end with a first thread pitch and a second threaded end with a second thread pitch. A core connects the first and second threaded ends. When the implant is implanted into a joint and rotated about its longitudinal axis when mated with a driver, a target joint may be compressed using the first thread pitch on a distal bone in the joint and the second thread pitch on a proximate bone in the joint. The first and second thread pitches may be the same but in opposing directions, may be different but in the same direction, or may be different and in opposing directions.

DOUBLE THREAD HAMMERTOES COMPRESSION DEVICE**FIELD OF DISCLOSURE**

[0002] The disclosed device and method generally relate to hammertoe correction implants and devices.

BACKGROUND

[0003] A hammertoe or contracted toe is a deformity of the proximal inter-phalangeal joint of the second, third, or fourth toe causing it to be permanently bent and giving it a semblance of a hammer. Initially, hammertoes are flexible and may be corrected with simple measures but, if left untreated, hammertoes may require surgical intervention for correction. Persons with hammertoe may also have corns or calluses on the top of the middle joint of the toe or on the tip of the toe and may feel pain in their toes or feet while having difficulty finding comfortable shoes.

[0004] Various treatment strategies are available for correcting hammertoes. Conventionally, the first line of treatment for hammertoes includes employing new shoes having soft and spacious toe boxes. Additionally, toe exercises may be prescribed to stretch and strengthen respective muscles, e.g., gently stretching one's toes manually, using the toes to pick up things off the floor, etc. Another line of treatment may include employing straps, cushions or non-medicated corn pads to relieve symptoms. An addition method of treatment may include correction by surgery if other non-invasive treatment options fail. Conventional surgery usually involves inserting screws, wires or other similar implants in toes to straighten them. Traditional surgical methods generally include the use of Kirschner wires (K-wires). Due to various disadvantages of using K-wires, however, compression screws are being employed as a better implant alternative as K-wires require pins protruding through the end of respective toes due to their temporary nature. As a result, K-

wires often lead to pin tract infections, loss of fixation, and other conditions. Additional disadvantages of K-wires include migration and breakage of the K-wires thus resulting in multiple surgeries.

[0005] Screw implants, however, may provide a more permanent solution as such implants do not need removal and thus have no protruding ends. Further, with the use of screw implants, a patient may wear normal footwear shortly after the respective surgery. Conventional screw implants possess a completely threaded body and do not provide a flexibility to the respective toe in its movement, i.e., conventional implants provide a pistoning effect. Furthermore, conventional screw implants are made for strong bones and are unsuitable for treatment of patients having weak bones which is a predominant reason why K-wire surgical implants are still employed despite their several disadvantages. Accordingly, there remains a need for developing hammertoe implants and devices including compression screw which are not only stable but provide adequate compression across a joint.

BRIEF DESCRIPTION OF THE DRAWINGS

[0006] Other objects, features, and advantages of the present invention will be apparent from the following description when read with reference to the accompanying drawings. In the drawings, wherein like reference numerals denote corresponding parts throughout the several views.

[0007] Figure 1 illustrates a front plan view of an exemplary implant according to some embodiments of the present subject matter.

[0008] Figure 2 is an illustration of an exemplary driver according to some embodiments of the present subject matter.

[0009] Figure 3 is an illustration of the drilling of the middle and proximal phalanxes of the foot.

[0010] Figure 4 is an illustration of the installation of an exemplary implant into a proximal phalanx of the foot.

[0011] Figure 5 is an illustration of the passing of the driver through the middle and distal phalanxes of the foot.

[0012] Figure 6 is an illustration of alignment of the middle, proximal and distal phalanxes of the foot with a re-engagement of the driver to an installed implant.

DETAILED DESCRIPTION

[0013] With reference to the figures, where like elements have been given like numerical designations to facilitate an understanding of the present subject matter, the various embodiments of a double thread hammertoe compression device are described.

[0014] It should be noted that the figures are not necessarily to scale and certain features may be shown exaggerated in scale or in somewhat schematic form in the interest of clarity and conciseness. In the description, relative terms such as “horizontal,” “vertical,” “up,” “down,” “top” and “bottom” as well as derivatives thereof (e.g., “horizontally,” “downwardly,” “upwardly,” etc.) should be construed to refer to the orientation as then described or as shown in the drawing figure under discussion. These relative terms are for convenience of description and normally are not intended to require a particular orientation. Terms including “inwardly” versus “outwardly,” “longitudinal” versus “lateral” and the like are to be interpreted relative to one another or relative to an axis of elongation, or an axis or center of rotation, as appropriate. Terms concerning attachments, coupling and the like, such as “connected” and “interconnected,” refer to a relationship wherein structures are secured or attached to one another either directly or indirectly through intervening structures, as well as both movable or rigid attachments or relationships, unless expressly described otherwise. When only a single machine is illustrated, the term “machine” shall also be taken to include any collection of machines that individually or jointly execute a set (or multiple sets) of instructions to perform any one or more of the methodologies discussed herein. The term “operatively connected” is such an attachment, coupling or connection that allows the pertinent structures to operate as intended by virtue of that relationship. In the claims, means-plus-function clauses, if used, are intended to cover the structures described, suggested, or rendered obvious by the written description or drawings for performing the recited function, including not only structural equivalents but also equivalent

structures. The terms “implant” and “device” are used interchangeably in this disclosure and such use should not limit the scope of the claims appended herewith.

[0015] Embodiments of the present subject matter provide a surgeon stability and compression across proximal or distal interphalangeal joints while maintaining simplicity of a hammertoe fusion. Exemplary embodiments may feature a double-ended threaded device, each end having a pitch (disparate or otherwise) that, when implanted, provides compression across a targeted joint.

[0016] Figure 1 illustrates a front plan view of an exemplary implant according to some embodiments of the present subject matter. With reference to Figure 1, an implant 100 for correcting hammertoes may comprise a proximal end 110 and a distal end 120 connected by a solid core 130 or rod. The proximal end 110 includes threads 112 on an external surface thereof having a first pitch, and the distal end 120 includes threads 122 on an external surface thereof having a second pitch. In one embodiment, the threads 112 on the proximal end 110 have a pitch of .039, and the threads 122 on the distal end 120 have a pitch of .049. Of course, these pitches are exemplary only and should not limit the scope of the claims appended herewith as the first and second thread pitches may be the same as each other and may be greater or lesser than the examples provided. Further, the thread pitches may be threaded in substantially the same direction or in opposing directions and may or may not have different pitches. The implant 100 may be constructed of any suitable material such as stainless steel, titanium, or other metals or rigid polymers. In one embodiment, the distal end 120 may include a female depression 125 adaptable to mate with a driver (not shown) having a male extension. Of course, the distal end 120 may have any suitable type of interfacing mechanism to accept conventional implant drivers such as a screw head or the like. For example, the distal end 120 may have a portion in the shape of a hex whereby a suitable driver has a corresponding hex adapter appropriate to drive the implant 100 into a respective bone.

[0017] Exemplary implants 100 may be implanted into targeted bones by conventional methods. For example, an exemplary implant 100 may be implanted or installed via a retrograde approach between, for example, proximate and middle phalanxes in a foot. One skilled in the art will understand that the method described herein may be

applied to the middle and distal phalanxes as well or other adjacent bones. Figure 2 is an illustration of an exemplary driver according to some embodiments of the present subject matter. With reference to Figure 2, an exemplary driver 200 may be an elongated instrument and include one end having an adaptable portion 210 suitable for mating with an implant 100 described above. In the illustrated example, the adaptable portion 210 comprises a male hexagonal head adaptable to mate to a corresponding female depression in an implant. In one embodiment of the present subject matter, the male hexagonal head is a 2.0 mm hexagonal head. Of course, other geometries and interfacing mechanisms are envisioned and the male hexagonal head of the driver 200 and its noted dimensions should not limit the scope of the claims appended herewith. On an opposing end of the driver 200 may be a driving pin 220 or trocar and may include a flat modular section 230 adaptable to accept a handle or other suitable mechanism to assist a surgeon during installation of an exemplary implant 100.

[0018] Figures 3-6 illustrate an exemplary method of installation or implantation of an implant according to embodiments of the present subject matter. With reference to Figures 3-6, in one embodiment to install an implant a toe 300 may be opened to provide access to a joint 302 between a middle phalanx 304 and a proximal phalanx 306. The middle and proximal phalanxes 304, 306, respectively, may be resected using a bone saw or other tool 350, if necessary. An intermedullary canal 320 may be drilled into both the middle and proximal phalanxes 304, 306 using a drill 350 or other mechanism to an appropriate depth. A driver 200 may be engaged with the distal end 120 of an exemplary implant 100 as described above, and the proximal end 110 of the implant 100 may be threaded into the proximal phalanx 306 until the threads of the distal end 120 of the implant sits flush to the surface of the proximal phalanx 306. The driver 200 may then be loosened and removed from the implant 100 and the driver retrograded distally until the pin or trocar end of the driver 200 passes through the middle phalanx 304 and out of the distal tip of the distal phalanx 308 as illustrated in Figure 5. The retrograde of the driver 200 may terminate when the adaptable portion of the driver 200 reaches the surface of the middle phalanx 304. The joint 302 may then be closed and the driver 200 re-engaged with the distal end 120 of the implant. Upon engagement of the driver 200 with the implant 100 the implant may be driven distally into the middle phalanx 304. As the distal end 120 of the implant 100 is

driven, i.e., rotated about its respective longitudinal axis, into the middle phalanx 304, compression of the respective joint 302 is created by the distal threads of the implant travelling faster than the proximal threads of the implant. Compression of the joint may also be effected as a function of the disparate thread pitches of the implant and/or the directions of the thread pitches of the implant.

[0019] Although reference has been made to a patient's proximal and distal interphalangeal joints metatarsal phalangeal joint, one skilled in the art will understand that embodiments of the present subject matter may be implemented for other respective bones including, but not limited to other phalanges/digits and phalangeal/digital joints.

[0020] It may be emphasized that the above-described embodiments, particularly any "preferred" embodiments, are merely possible examples of implementations and merely set forth for a clear understanding of the principles of the disclosure. Many variations and modifications may be made to the above-described embodiments of the disclosure without departing substantially from the spirit and principles of the disclosure. All such modifications and variations are intended to be included herein within the scope of this disclosure and the present disclosure and protected by the following claims.

[0021] While this specification contains many specifics, these should not be construed as limitations on the scope of the claimed subject matter, but rather as descriptions of features that may be specific to particular embodiments. Certain features that are described in this specification in the context of separate embodiments can also be implemented in combination in a single embodiment. Conversely, various features that are described in the context of a single embodiment can also be implemented in multiple embodiments separately or in any suitable sub-combination. Moreover, although features may be described above as acting in certain combinations and even initially claimed as such, one or more features from a claimed combination can in some cases be excised from the combination, and the claimed combination may be directed to a sub-combination or variation of a sub-combination.

[0022] As shown by the various configurations and embodiments illustrated in Figures 1-6, a double thread hammertoe compression device has been described.

[0023] While preferred embodiments of the present subject matter have been described, it is to be understood that the embodiments described are illustrative only and that the scope of the invention is to be defined solely by the appended claims when accorded a full range of equivalence, many variations and modifications naturally occurring to those of skill in the art from a perusal hereof.

We Claim:

1. A bone implant comprising:

an elongated device having a first threaded end with a first thread pitch and a first thread direction, and

a second threaded end with a second thread pitch, a second thread direction opposite the first thread direction of the first threaded end, and a depression adapted to accommodate a driver; and

a core monolithically connecting the first and second threaded ends,

wherein the implant is configured to be implanted into a joint, and

wherein, when the implant is rotated in a first rotation direction about its longitudinal axis after being mated with the driver, the joint is compressed first threaded end is inserted into a proximal using the first thread pitch on a distal bone in the joint using the first thread pitch and the first thread direction, and

wherein, when the implant is rotated in a second rotation direction about its longitudinal axis opposite the first rotation direction while being mated with the driver, the second threaded end is inserted into a distal bone in the joint such that the joint is compressed using the first and second thread pitches and the first and second thread directions on a proximate distal bone in the joint.

2. The bone implant of Claim 1, wherein the first thread pitch is 0.039 millimeters.

3. The bone implant of Claim 1 or 2, wherein the second thread pitch is 0.049 millimeters.

4. The bone implant of Claim 1, 2 or 3, wherein the first and second thread pitches are different and in opposing directions thread pitch is less than the second thread pitch.

5. The bone implant of any one of Claims 1 to 4 wherein the distal bone is a phalange selected from the group consisting of proximal phalange, intermediate phalange, distal phalange, and combinations thereof.

6. The bone implant of any one of Claims 1 to 5, wherein the proximal bone is a phalange selected from the group consisting of proximal phalange, intermediate phalange, distal phalange, and combinations thereof.

7. A system for correcting toe deformities, comprising:

a monolithic bone implant elongated along a longitudinal axis, the bone implant comprising a first threaded end with a first thread pitch and a first thread direction, and a second threaded end with a second thread pitch and a second thread direction opposite the first thread direction, and wherein the first and second threaded ends are interconnected by a core; and

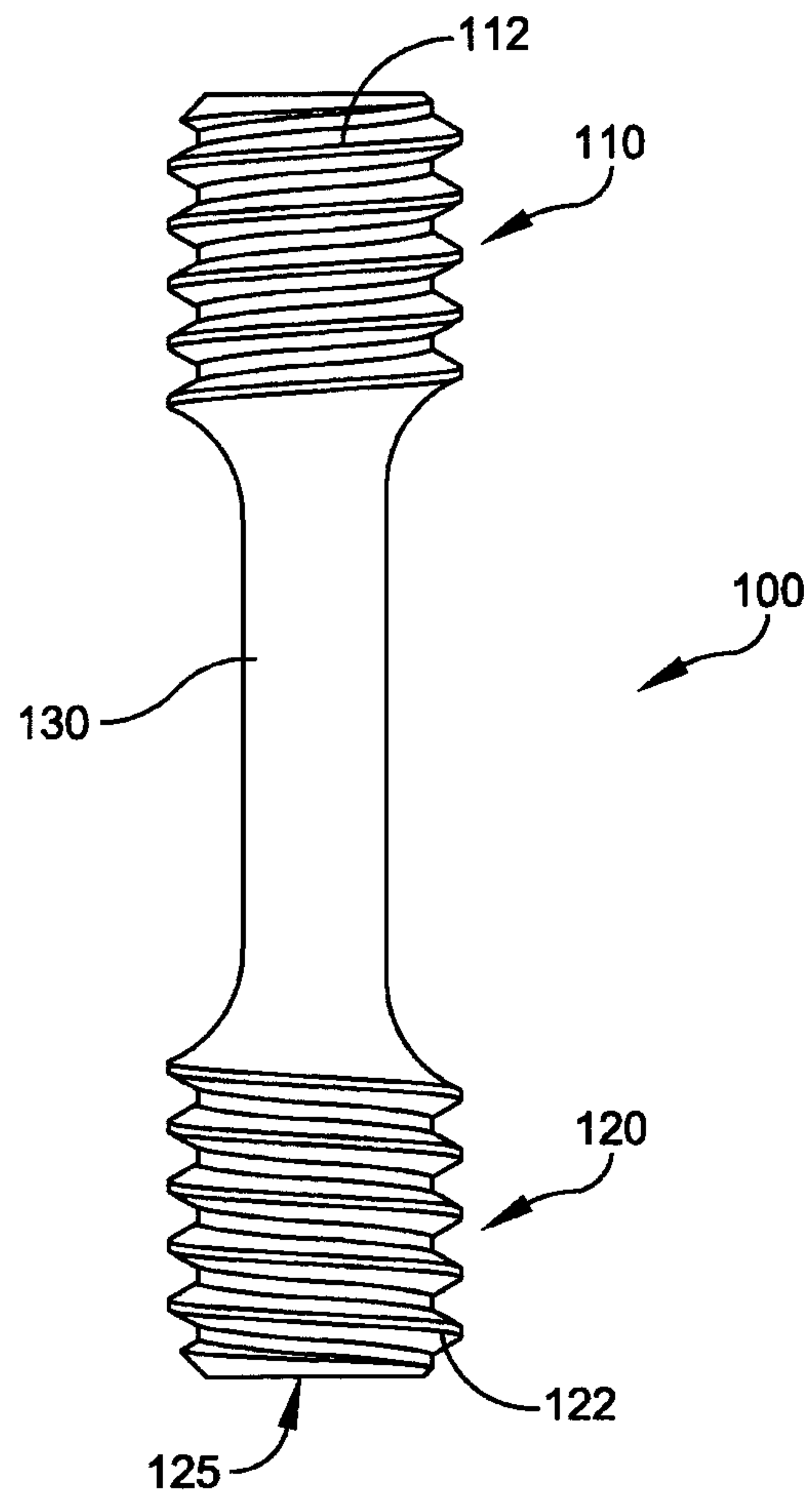
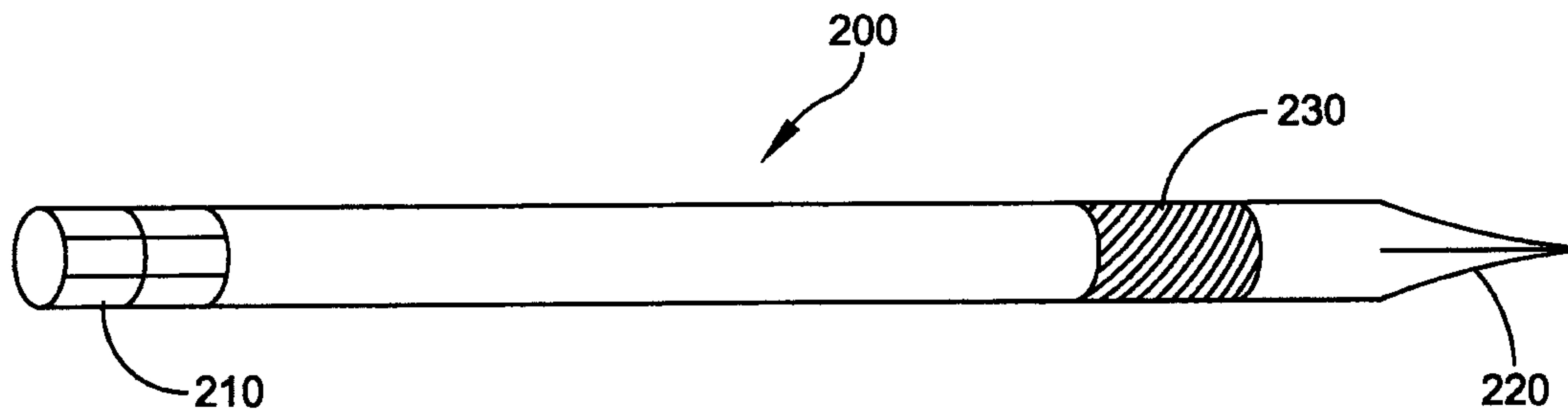
a driver configured to engage the second threaded end of the implant, rotate the implant about its longitudinal axis in a first rotation direction to insert the first threaded end into a proximal bone of a joint using the first thread pitch and the first thread direction, and rotate the implant about its longitudinal axis in a second rotation direction opposite the first rotation direction to insert the second threaded end into a distal bone in the joint such that the joint is compressed using the first and second thread pitches and the first and second thread directions.

8. The system of Claim 7, wherein the second threaded end has a female depression head adapted to accommodate the driver.

9. The system of Claim 7 or 8, wherein the first thread pitch is less than the second thread pitch.

10. The use of the bone implant of any one of Claims 1 to 6 for connecting hammertoes.

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**Figure 1****Figure 2**

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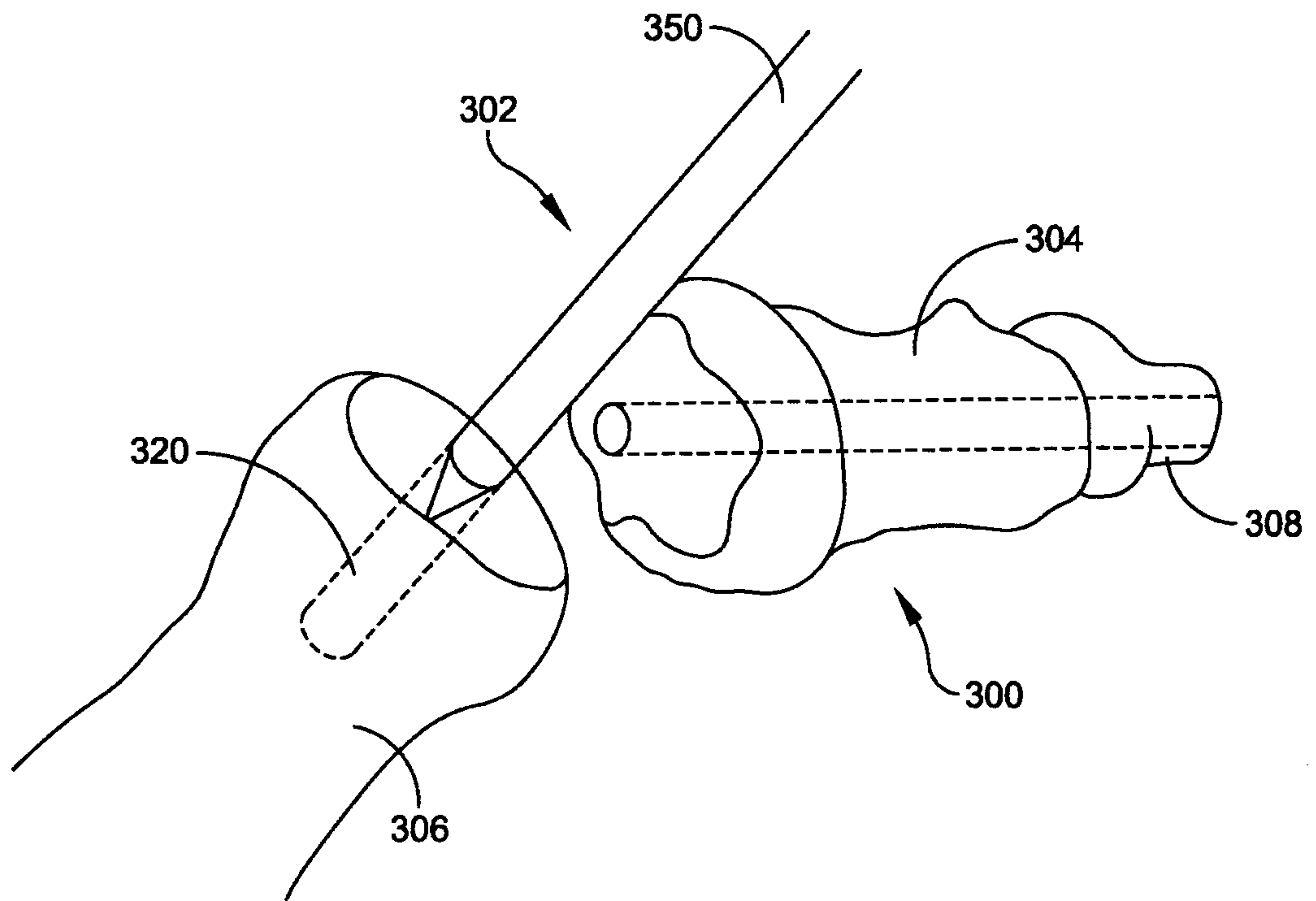


Figure 3

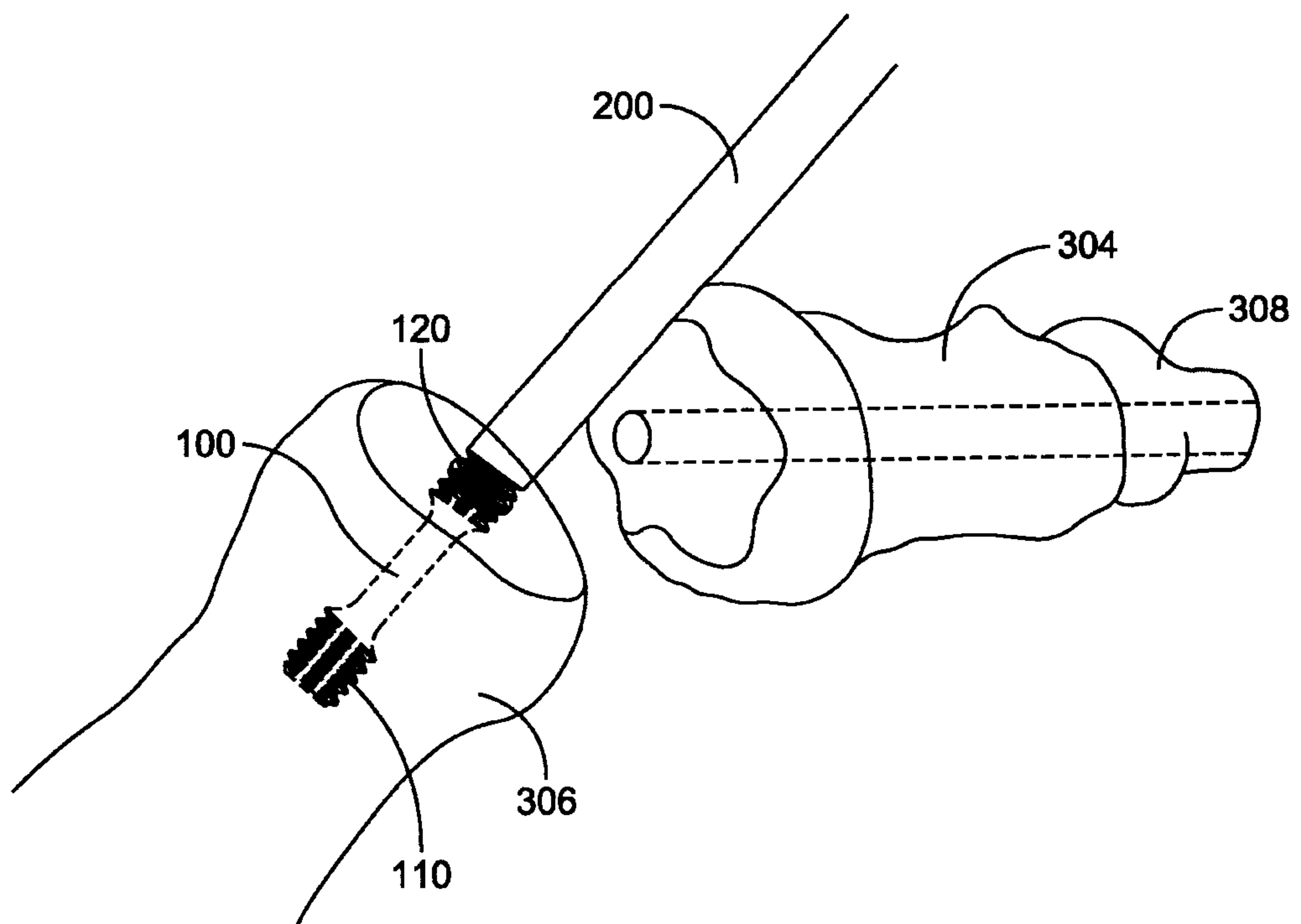


Figure 4

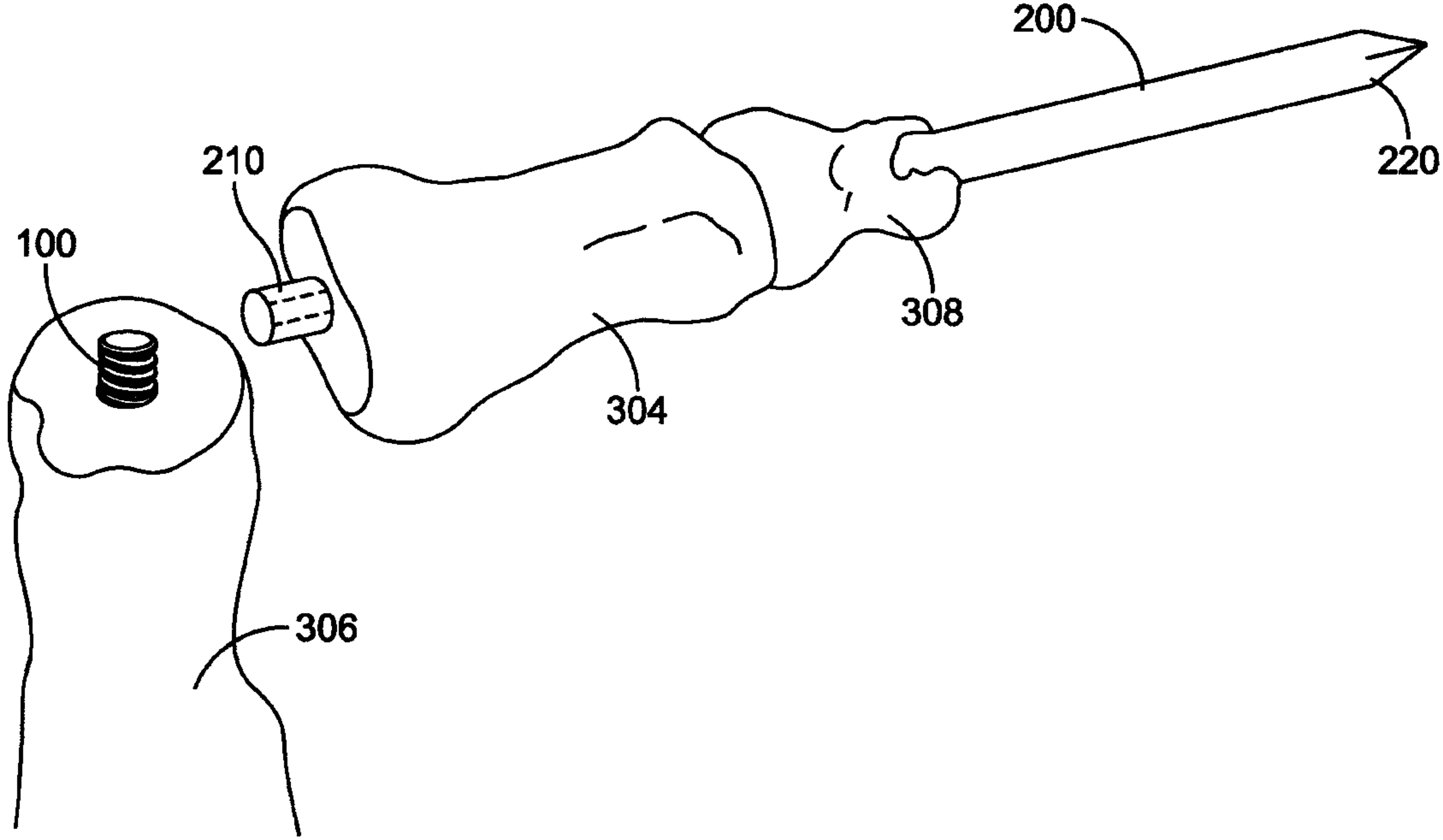


Figure 5

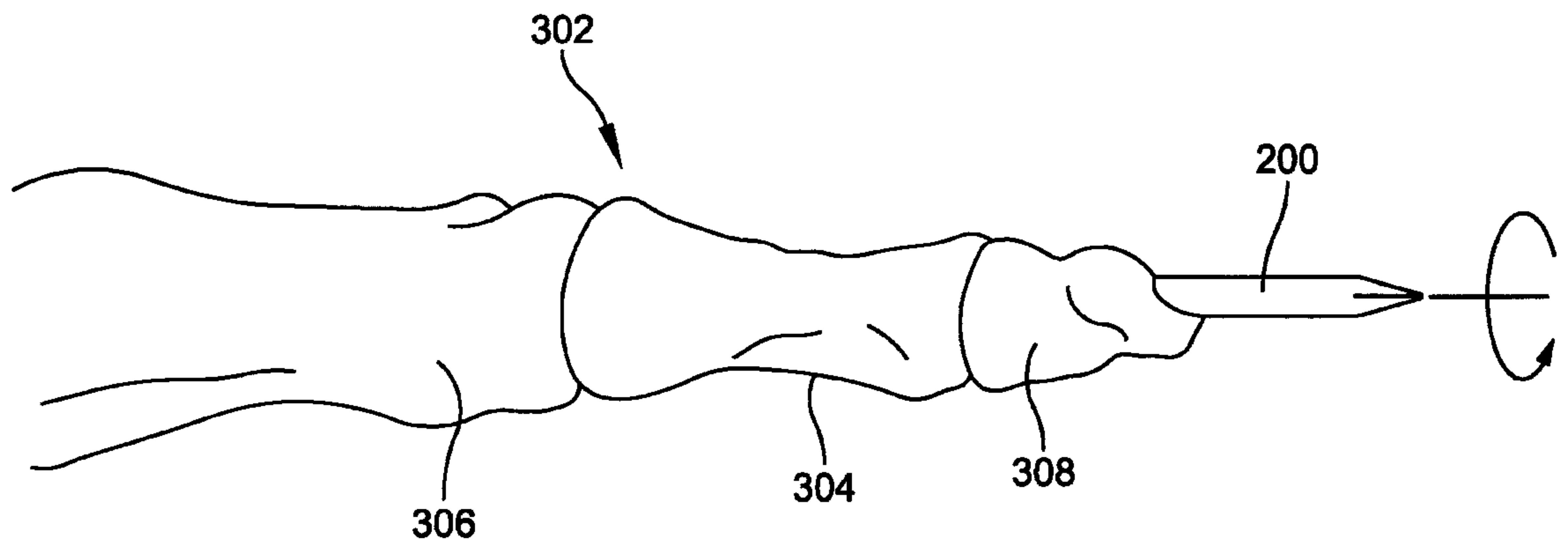


Figure 6

