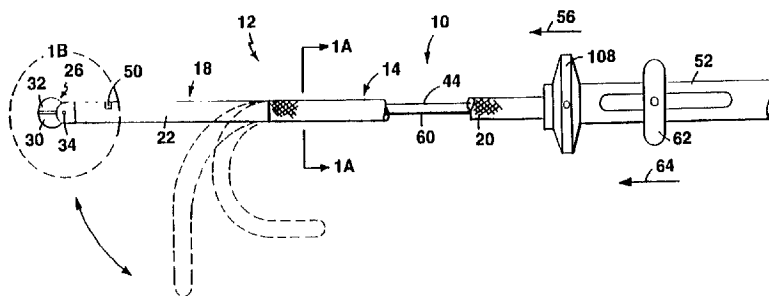




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(54) **CATHETER ORIENTABLE POUR BIOPSIE**  
(54) **DEFLECTABLE BIOPSY CATHETER**



(57) Ce cathéter orientable (10) pour biopsie permettant d'obtenir un échantillon de tissu d'une cavité du corps d'un patient comprend une tige de cathéter allongée (12), un fil métallique (44) pour orienter la tige, une paire de mâchoires (30)(32) et un fil métallique d'actionnement (60). On décrit également un procédé permettant d'effectuer une ablation de tissu ou une électrocoagulation.

(57) A deflectable biopsy catheter (10) for obtaining a tissue sample from a body cavity of a patient comprises an elongated catheter shaft (12), a deflection wire (44), a pair of jaws (30, 32), and an actuation wire (60). Treating tissue by ablation or electro-coagulation are also disclosed.

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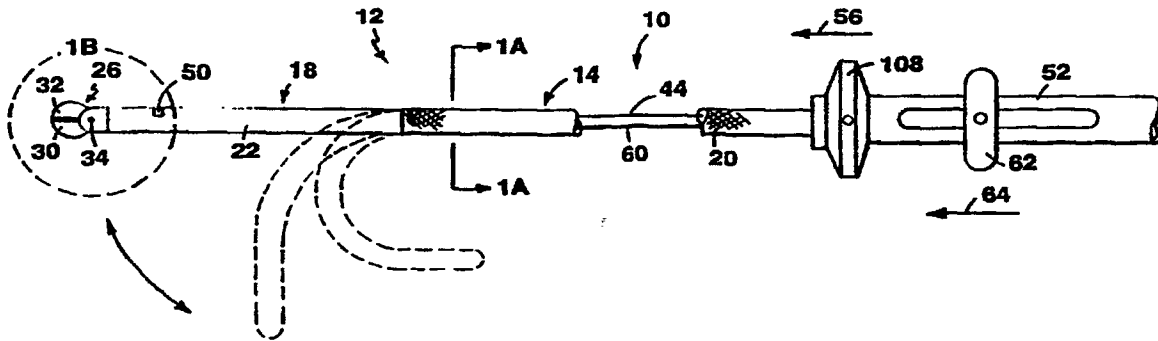
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## (57) Abstract

A deflectable biopsy catheter (10) for obtaining a tissue sample from a body cavity of a patient comprises an elongated catheter shaft (12), a deflection wire (44), a pair of jaws (30, 32), and an actuation wire (60). Treating tissue by ablation or electro-coagulation are also disclosed.

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## DEFLECTABLE BIOPSY CATHETER

Background

This invention relates to a deflatable biopsy  
5 catheter.

Biopsy is a commonly performed surgical procedure  
in which tissue samples are obtained for diagnostic  
purposes. Such a procedure requires cutting a tissue  
sample and then retrieving the cut sample. In this  
10 application, sampling forceps are typically carried on  
the distal end of a catheter and positioned around a  
tissue portion selected for removal and diagnosis. The  
sampling forceps cut the selected tissue and retain the  
sample so that it is removed from the patient's body  
15 along with the catheter.

Summary

In a first aspect, the invention features a  
deflatable biopsy catheter for obtaining a tissue sample  
from a body cavity of a patient comprising: an axially  
20 elongated catheter shaft having proximal and distal  
portions respectively terminating at proximal and distal  
ends, the catheter shaft being sized and constructed to  
be advanced into a body cavity of a patient; a deflection  
wire coupled to the distal portion of the catheter shaft  
25 and extending within the catheter to the proximal end  
thereof; and a pair of biopsy jaws coupled to the distal  
end of the catheter shaft and having first and second  
opposed free cutting surfaces exposable for contact with  
a selected area of tissue within the patient's body  
30 cavity and movable with respect to each other to cut a  
tissue sample from the selected area of tissue.

Embodiments may include one or more of the  
following features. The biopsy jaws are preferably  
formed of hollow cup-shaped members that are pivotally  
35 hinged together about a pivot bearing coupled to the  
distal end of the catheter shaft. An axially elongated

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actuation wire is preferably coupled to the biopsy jaws and extending proximally therefrom to the proximal end of the catheter shaft, the actuation wire being constructed and arranged to selectively move the jaws. A tracking  
5 member is preferably coupled to the deflection wire and is preferably constructed and arranged to track movement of the actuation wire and to couple tension on the actuation wire to the deflection wire to counteract force applied by the actuation wire to the distal portion of  
10 the catheter during movement of the jaws. The deflection wire and the actuation wire are preferably arranged on radially opposed sides of the catheter axis in the distal portion of the catheter shaft. The distal portion of the catheter shaft preferably defines first and second non-  
15 coaxial lumens: the first and second lumens being radially offset from the axis of the catheter shaft and the deflection wire being disposed in the first radially offset lumen and the actuation wire being positioned in the second radially offset lumen. The opposed jaws are  
20 preferably formed from electrically conducting material and together form a generally dome-shaped outer electrically conducting surface.

In some embodiments, the cutting surfaces of the biopsy jaws preferably comprise a plurality of serrated  
25 teeth for cutting body tissue. Some embodiments include a needle coupled to the distal end of the catheter shaft and constructed and arranged to penetrate heart tissue to a selected depth. Embodiments suited for use in the heart include biopsy jaws that respectively include  
30 hollow cup-shaped distal sections for cutting tissue coupled to solid proximal sections having flat surfaces exposable for contact with tissue for ablation. The cup-shaped portions are preferably electrically insulated from the ablation electrode sections.

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In another aspect, the invention features a scheme for obtaining a tissue sample from a body cavity of a patient comprising the steps of: advancing a deflectable biopsy catheter, as defined above, within a body cavity  
5 of a patient; steering the catheter through the patient's body cavity and to a selected portion of body tissue by selectively deflecting the distal end of the catheter by applying tension to the deflection wire; opening the opposed jaws in the vicinity of the selected  
10 portion of body tissue; torquing the catheter shaft and deflecting the distal end of the catheter so that the opposed jaws are positioned about the selected portion of body tissue; and closing the jaws to cut a sample of tissue from the selected portion of body tissue.

15 In some embodiments, the opposed biopsy jaws together form an exposed electrically conductive surface and the selected area of heart tissue is electro-coagulated by supplying to the electrically conductive surface formed by the biopsy jaws energy sufficient to  
20 achieve tissue electro-coagulation. The distal portion of the catheter is preferably deflected to increase pressure applied by the exposed conductive surface of the biopsy jaws against the selected portion of tissue during electro-coagulation.

25 In another aspect, the invention feature a scheme for obtaining a tissue sample from the heart of a patient comprising the steps of: advancing a deflectable biopsy catheter, as defined above, through the vasculature of a patient, wherein the opposed biopsy jaws together form an  
30 exposed electrically conductive electrode surface and further comprising a second electrically conductive electrode surface; steering the catheter through the vasculature and into the heart of the patient by deflecting the distal end of the catheter by applying  
35 tension to the deflection wire; selecting the area of

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heart tissue to be diagnosed based on measurements of electrical potentials within the patient's heart between the first and second electrode surfaces; opening the opposed jaws in the vicinity a selected portion of heart tissue; torquing the catheter shaft and deflecting the distal end of the catheter so that the opposed jaws are positioned about the selected portion of heart tissue; and closing the jaws to cut a sample of tissue from the selected portion of heart tissue.

10 In some embodiments, the area of heart tissue to be ablated is selected based on measurements of electrical potentials within the heart between the first and second electrode surfaces. In some cases the area of heart tissue selected to be ablated is ablated by  
15 supplying to the electrically conductive surface formed by the biopsy jaws energy sufficient to achieve tissue ablation.

Embodiments may include one or more of the following advantages. The ability to deflect the  
20 catheter enables an operator to precisely position the biopsy jaws within a body cavity of a patient (e.g., around interfering anatomical body features). The catheter allows an operator to close the biopsy jaws onto a tissue sample without displacing the position of the  
25 catheter tip. This increases the reliability of the procedure and decreases the overall procedure time, increasing safety and patient comfort. In addition, by deflecting the distal tip of the catheter, the pressure of the biopsy jaws against the tissue to be cut is  
30 increased, improving the ability to take samples and improving the uniformity and the effectiveness of tissue electro-coagulation. The catheter achieves high torque transmission without sacrificing flexibility of the catheter shaft, so that the catheter may easily follow  
35 the inherent tortuosity of a patient's anatomy without

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risk of injury to the patient. This permits an operator to precisely control the position of the catheter tip during advancement of the catheter through the body. The deflectability and steerability of the catheter enable  
5 the biopsy catheter to be advanced within a patient's body with or without the assistance of an endoscope or the like. The multi-modality features of the catheter suited for use in the heart enhances an operator's ability to treat and diagnose the condition of a  
10 patient's heart.

Other features and advantages of the invention will become apparent from the following.

#### Description

Fig. 1 is a diagrammatic side view of a  
15 deflectable biopsy catheter.

Fig. 1A is a cross sectional view of the body of the catheter shown in Fig. 1 taken along the line 1A-1A.

Fig. 1B is an enlarged side view, in partial cross section, of the distal tip of the catheter of Fig. 1.

20 Fig. 1C is a cross sectional view of the catheter tip shown in Fig. 1B taken along the line 1C-1C.

Fig. 1D is a diagrammatic front view of the distal end of the catheter shown in Fig. 1B with the jaws fully open.

25 Fig. 2 is a diagrammatic cross-sectional side view of the distal tip of the catheter of Fig. 1.

Fig. 3 is a diagrammatic side view, in partial cross section, of the proximal end portion of the catheter of Fig. 1.

30 Fig. 3A is a cross sectional view of the proximal end of the catheter shown in Fig. 3 taken along the line 3A-3A.

Fig. 3B is a cross sectional side view of the proximal end of the catheter shown in Fig. 3.

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Fig. 3C is a diagrammatic top view of a lock mechanism in the proximal end of the catheter shown in Fig. 3.

5 Figs. 4 and 4A are diagrammatic side views of the catheter of Fig. 1 disposed within a body cavity of a patient for obtaining a tissue sample.

Fig. 5 is a diagrammatic side view, in partial cross section, of the distal end of an alternative deflectable biopsy catheter.

10 Fig. 6 is a diagrammatic side view, in partial cross section, of the distal end of an alternative deflectable biopsy catheter.

Fig. 7 is a diagrammatic cross-sectional side view of a deflectable biopsy ablation catheter.

15 Fig. 7A is a diagrammatic end view of the catheter of Fig. 7.

Fig. 8 is a diagrammatic view of the catheter of Fig. 7 disposed within the vasculature of a patient.

20 Fig. 8A is a diagrammatic side view of the distal end of the catheter of Fig. 7 measuring electrical potentials within the heart of a patient.

Fig. 8B is a diagrammatic side view of the distal end of the catheter of Fig. 7 positioned to take a sample within the heart of a patient.

## 25 Structure

Referring generally to Figs. 1-1D, a deflectable biopsy catheter 10 includes an elongated catheter shaft 12 that has a relatively stiff hollow catheter body 14 that defines a lumen 16 and is bonded to a relatively flexible, deflectable distal tip 18. The catheter body includes a braided shaft 20. The distal tip of the catheter is formed from a short section of flexible tubing 22 that is preferably more flexible than the catheter body. The proximal end of the distal tip of the



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catheter includes a circumferential notch 24 (Fig. 1B) that has an outer diameter selected to snugly fit within the distal lumen of catheter body 14. The catheter tip is bonded to the catheter body using a conventional

5 adhesive.

As shown in greater detail in Fig. 1B, catheter 10 further has a biopsy sampler 26 that is mounted on catheter tip 18. Biopsy sampler 26 is formed from two opposed jaws 30, 32 that are hinged together and movable  
10 with respect to each other, about a pivot bearing 34, into a closed position (shown by solid lines) and into an open position (shown by dashed lines). The jaws are formed into hollow hemispherical or cup-shaped members that have respective circumferential free cutting edges  
15 28, 29 that cooperate with each other to cut tissue when the jaws are closed. The jaws, when closed, together form a dome-shaped outer surface that is exposed for contact with body tissue and that may be constructed for electro-coagulation. A rubber seal 38 prevents the  
20 seepage of blood and other body fluids into the catheter through the distal end of the device.

Distal tube 22 defines a pair of non-coaxial lumens 40, 42. A deflection wire 44 extends into lumen 40 to a position near the distal end of the catheter  
25 where it is crimped onto a stainless steel hypotube 46 which is welded to a short length (e.g., 0.2 inches) of stainless steel ribbon 48 to form a "T" structure. The ribbon sits within an opening 50 in the wall of the catheter tip. The ribbon is larger than opening 50. The  
30 ribbon is bonded to the catheter tip by filling the opening with a biocompatible adhesive. Deflection wire 44 is coupled from the catheter tip to a piston 52 which is slidably disposed within a bore of a control handle 54. The catheter tip is deflected by gripping the  
35 control handle housing and moving the piston distally

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(shown by arrow 56) out of the piston chamber, which  
tenses the deflection wire and draws the distal end of  
the catheter proximally toward the handle. Because the  
deflection wire is attached to one side of the catheter  
5 tip, the tip preferentially bends radially in the  
direction of attachment (shown in phantom in Fig. 1).

The deflection wire is preferably surrounded by  
a teflon sheath that extends from a location near the  
proximal end of the piston chamber to a distal location  
10 that is spaced proximally of the distal end of the  
deflection wire by at least a distance equal to the  
maximum operating length of longitudinal movement of the  
piston relative to the housing (e.g.,  $\frac{1}{2}$  to  $\frac{3}{4}$  inch). The  
sheath provides lubricity for the movement of the  
15 deflection wire, and also serves to maintain the  
deflection wire in generally coaxial relation with the  
catheter body 14. The deflection wire is maintained in  
coaxial relation with the catheter body so that the  
length of the deflection wire and the on-axis length of  
20 the catheter body are substantially the same, whether the  
catheter body extends around a curve or not. In this  
arrangement, less energy is required for rotation of the  
catheter tip. This allows the tip to be more responsive  
to rotation of the handle and therefore more easily  
25 controlled.

As shown in Fig. 1, an actuation wire 60 is  
coupled between the jaws and an actuation knob 62 at the  
proximal end of the catheter. The jaws are opened when  
the actuation knob is moved in the distal direction  
30 (shown by arrow 64), and the jaws are closed when the  
actuation knob is move in the opposite direction. The  
diameter and the constituent material of the actuation  
wire are selected so that the actuation wire has  
sufficient axial stiffness to support the axial load  
35 necessary to open the jaws. In a presently preferred

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embodiment, the actuation wire is formed from conductive material (e.g., nitinol) and serves to deliver rf electro-coagulation energy to the jaws.

As shown in Fig. 2, in a presently preferred  
5 embodiment, jaws 30, 32 include respective proximal extensions 66, 68 onto which are looped respective wire strands 70, 72. The length of strand 70 is made longer than the length of strand 72, as shown. Strands 70, 72 are wound together and are coupled to actuation wire 60  
10 by a crimp junction 74. Actuation wire 60 and deflection wire 44 are respectively disposed in the non-coaxial lumens 40, 42 so that when the jaws are closed, proximally-directed tension, applied by actuation wire 60 to the catheter tip (urging displacement of the position  
15 of the catheter tip), is substantially counteracted by application of proximally-directed tension to deflection wire 44, as described below in connection with Fig. 3B. The radial position of the actuation wire relative to the central axis of the catheter tip is adjusted to achieve  
20 the desired compensation effect (e.g., by changing the radial position and the size of lumen 42).

Referring to Fig. 3, control handle 54 includes a cylindrical housing 76 that has a cylindrical bore 78. Piston 52 has a distal end that is attached to the  
25 proximal end of the catheter shaft and a proximal end that is slidably disposed within the bore of housing 76. The proximal end of catheter body 14 fits within a bore defined by piston 52 and abuts against a lip region of the piston where the diameter of the piston bore is  
30 reduced. The catheter body is attached at the proximal end to the piston using, e.g., a cyanoacrylate adhesive.

As shown in Figs. 3A and 3B, actuation knob 62 is mounted onto a slide bar 80 which freely slides within a slot 82 in piston 52. Slot 82 has a hole 84 through  
35 which deflection wire 44 passes and a hole 86 at which

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the proximal end of the actuation wire is attached, e.g., by a solder crimp joint 88. A tracking device 90 (e.g., a stop) is attached to deflection wire 44 so that when the actuation knob is moved in the proximal direction to close the jaws, the stopper is engaged by slide bar 80, which exerts tension on the deflection wire to compensate for the forces applied by the actuation wire that act to displace the position of the catheter tip. Thus, the tracking member tracks movement of the actuation wire and couples tension applied to the actuation wire to the deflection wire for counteracting force applied by the actuation wire to the distal portion of the catheter.

Referring back to Fig. 3, the handle housing is generally symmetrical about its longitudinal axis, allowing the handle to be freely rotated by an operator. The piston includes a circumferential O-ring notch 92 that carries an O-ring 94 to provide a watertight seal between the piston and the wall of the piston chamber. The piston includes a first slot 96 that extends along a portion of its length proximal of the o-ring notch. A set screw 98 extends from the wall of the housing into the slot. Slot 96 includes a keyway lock profile 100 (Fig. 3C). The set screw restricts the longitudinal movement of the piston by engaging the walls 102 of the keyway lock profile. To steer the catheter tip, the piston is pushed in and out of the slots 104, defined by the walls of lock profile 100, until a desired tip deflection is achieved. An annular thumbrest 108 is then twisted to lock the piston in place relative to the control handle housing.

A second slot 106 is disposed on the opposite side of the piston as the first slot. Within the second slot are two adjacent, short (e.g.,  $\frac{1}{8}$  inch long) pieces of teflon tubing that provide a lubricous surface to facilitate axial movement of the piston with respect to

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the handle housing. The distal end of the piston extends beyond the distal end of the housing so that it may be manually controlled by a user. Annular thumbrest 108 is attached to the distal end of the piston to facilitate axial movement of the piston.

Deflection wire 44 extends through the axial bore of the piston, through hole 84 in slide bar 80 to the proximal end of handle housing 76, where it is attached by an anchor 110. The anchor extends into a transverse hole in the portion of the housing between the connector and the piston chambers. The anchor is rotatable within the hole, but fits snugly so that it does not rotate freely. The anchor includes a transversely extending hole that may be rotated into alignment with the axis of the handle housing to receive the proximal end of the deflection wire. The anchor is rotated by means of a flat screw driver slot 112 to adjust the tension on the deflection wire.

Actuation wire 60 extends from the catheter body proximally through the axial bore of the piston to the proximal end of the control handle housing. A lead wire 113 is coupled to the actuation wire at the actuation knob to provide electrical energy to the actuation wire. At the proximal end of the handle housing the lead wire is bowed slightly to provide slack as the catheter is manipulated. The lead wire is connected to a plug 114 that extends proximally from the handle housing.

A closely wound spring coil 116 is disposed within the lumen of the catheter shaft. The coil extends distally from the proximal end of catheter body 14 to near the distal end of the catheter body. The coil structure efficiently transmits torque from the proximal end of the catheter to the catheter tip because the direction of the applied torque substantially corresponds to the incompressible axis of the coiled wire. In a

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presently preferred embodiment, the proximal end of the coil is securely attached to the proximal end of the catheter body, but the distal end of the coil is unattached to the catheter body. This allows a certain amount of stretch in the portion of the coils on the outside portion of a bent region of the catheter body, thereby achieving a high flexibility while providing the efficient torque-transmitting capability of the coil. In other words, as the catheter body is bent e.g., through the aortic arch, the upper part of the coil opens up to maintain the flexibility, but the inner portion of the coil is tight in compression. In this position, the coil, together with the catheter body, are able to transmit torsional and tensile forces exerted on the proximal end of the catheter. Further details regarding the arrangement of the coil and the catheter shaft are provided in U.S. Serial No. 08/138,863, filed October 19, 1993, which is herein incorporated by reference.

In a presently preferred embodiment, the jaws are made of stainless steel and are each roughly 4 mm in diameter (e.g., for electrophysiological procedures). The ring electrode is made of platinum and is about 1.3 mm wide. The actuation wire is made of nitinol and has a diameter of about 0.018-0.019 inch. The deflection wire is made of nitinol and has a diameter of about 0.01 inch. Typically a force of about 10-12 pounds is required to deflect the distal portion of the catheter by one hundred and eighty degrees. Preferably, the handle and piston are formed from acetal (e.g., DELRIN™). For cardiac sampling procedures, the length of the catheter shaft is about 48 inches (120 cm), while the length of the catheter tip is typically between 1½ and 3 inches (3.8-7.6 cm); the outer diameter of the catheter body is typically about 7 French (0.23 cm), and the outer diameter of the catheter tip is typically about 6 French

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(0.2 cm). The choice of the catheter dimensions, e.g., for other applications, will depend upon the anatomy of the patient and the type of procedure to be performed. The braided shaft is formed from counter-wound double  
5 stainless steel wires with a pick count (i.e., the number of times that wires cross a unit of tube length) of about thirty-two to thirty-four times per inch that are braided over a polyurethane tube which is over-extruded with a polyurethane coating that bonds through the braid to the  
10 inner tubing to form a unitary structure with a hardness of about D70. The distal portion of the catheter shaft is formed from a polyurethane extrusion and preferably has a hardness of about D60. The spring coil 72 has an inside diameter of about 0.038 inch (0.10 cm) and an  
15 outside diameter of about 0.058 inch (0.15 cm), and fits closely within the inside diameter of the shaft 30, which is about 0.059-0.062 inch (0.15-0.16 cm). The coil is made from e.g., #302 stainless steel wire that has a circular cross-section (although a wire with a  
20 rectangular cross-section may be used). The coil may be fabricated from other spring-like materials, such as nitinol.

During fabrication of catheter 10, catheter body  
14 slides over a tip assembly that includes catheter tip  
25 18 with the biopsy jaws, and the deflection and actuation wires. All of the wires are pulled through the catheter body. The spring coil slips over the proximal end of the deflection and actuation wire and into the catheter body. The proximal end of the catheter body is then attached to  
30 the distal end of the piston portion of the control handle.

#### Operation

Referring to Fig. 4, deflectable biopsy catheter 10, pushed through a working channel (typically having an  
35 inner diameter of about 2.8-4 mm) of an endoscope 115,

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enters a cavity within a patient's body (e.g., the gastrointestinal tract, the intestines, the uterus, the muscles, the bile duct, the heart, and the esophagus) to a location 117 identified as a potential abnormal tissue site. By torquing the catheter body and deflecting the catheter tip under fluoroscopic visualization, the catheter is steered around interfering anatomical features 118 within the body cavity to the abnormal site. During advancement of the catheter, the position of the endoscope is held steady to serve as a reference platform. We note that the deflectability and the steerability of catheter 10 allows an operator to advance the catheter within a patient's body without the assistance of an endoscope or the like.

Referring to Fig. 4A, upon achieving proper placement, the operator opens the jaws about the sampling site 117 by pressing forward on the actuation knob of the catheter. With the jaws fully open, the catheter tip is deflected by pushing distally on thumbrest 108 (indicated by arrow 56 in Fig. 1), which presses the jaws against the myocardial tissue, increasing the normal force 121 applied by the electro-coagulation surfaces of the jaws. The deflection of the catheter tip is locked in place by twisting the piston relative to the handle housing. The operator then moves the actuation knob in the proximal direction to close the jaws about the selected portion of tissue and to cut the tissue. The cut tissue is retained within the cavity defined by the jaws during removal of the catheter from the patient's body.

In some cases it may be necessary to prevent the sampled region of tissue from bleeding. In these cases, rf energy is delivered to the exposed, dome-shaped, electrically conductive outer surface formed by the jaws to electrically coagulate the tissue in the sampled region. For improved electro-coagulation, the catheter



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tip is deflected so that the dome-shaped electrode surface is pressed into the tissue in the sampled region. This increases the depth and the uniformity of electro-coagulation.

5 Other embodiments are within the scope of the claims.

Referring to Fig. 5, in an alternative embodiment, instead of flat surfaces, the exposable cutting surfaces of jaws 30, 32 include respective arrays of serrated  
10 teeth 130, 132 that mate together when the jaws are closed. Teeth 130, 132 provide additional cutting and tearing force for obtaining tissue samples.

Alternatively, as shown in Fig. 6, an axially oriented needle 140 is mounted on the distal end of the  
15 catheter. Needle 140 is constructed to penetrate tissue to a selected depth (e.g., 1-3 mm) beyond the proximal end of the jaws to facilitate fixation of the distal end of the catheter against body tissue, increasing the stability of the device and increasing the accuracy of  
20 the biopsy procedure. The needle preferably has an outer diameter of about 0.015 inch. In some embodiments, needle 140 is selectively extendable from and retractable into the catheter shaft.

In another embodiment, the biopsy jaws are  
25 electrically insulated from each other by forming pivot bearing 34 from electrically insulating material (e.g., DELRIN™) and by inserting electrically insulating material the exposed surfaces of the jaws. In operation, the jaws are opened and are positioned about a tissue  
30 sample. The biopsy jaws are then closed and a voltage is applied to the electrode surfaces of the jaws, creating an arc therebetween for cutting the tissue. The jaws are then completely closed to retain the cut sample within the cavity defined by the jaws.

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Referring to Figs. 7 and 7A, in another embodiment, deflectable biopsy catheter 150 includes two jaws 152, 154 designed for sampling cardiac tissue and for ablating arrhythmic tissue. Jaws 152, 154  
5 respectively include hollow cup sections 156, 158 and solid, flat ablation electrode sections 160, 162. The electrode sections are electrically insulated from the cup sections by insulating layers 164, 166 (e.g., made from teflon). Catheter 150 also includes at least one  
10 ring electrode 168 mounted on the catheter tip. An electrode lead wire 170 is coupled to the ring electrode and extends to the proximal end of the catheter to provide electrical communication with the ring electrode.

In a presently preferred embodiment, each jaw is  
15 made from stainless steel and is about 4 mm long by about 2 mm wide. When closed, the two jaws form a generally hemispherical cavity with a diameter of about 2 mm. When open, the exposed electrode surface area (corresponding to the flat surfaces of ablation electrode sections 160,  
20 162) is about 4 mm<sup>2</sup>.

Referring to Fig. 8, in an electrophysiology procedure, deflectable biopsy ablation catheter 150 is introduced through an introducer sheath into the right femoral artery of a patient 120 by use of the Seldinger  
25 technique (alternatively, the catheter may be introduced through the left femoral artery or through the right or left femoral vein, depending upon the region of the heart to be accessed). An operator advances the catheter under fluoroscopic guidance through the patient's vasculature  
30 by simultaneously deflecting the distal tip of the catheter and applying torque to the proximal end of the catheter. The catheter is advanced through the inferior vena cava until the catheter tip 18 is positioned in a chamber of the patient's heart 122 (e.g., in the right

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atrium 124). The catheter enters the right atrium in an undeflected state. The operator maneuvers steerable tip 18 around the anatomical structure of the heart to position the biopsy jaws into the region of the heart  
5 that is to be mapped or ablated (e.g., the right ventricle 126). Thus, the deflectability of the catheter permits the operator to accurately position the electrodes against the desired portion of the heart wall.

Referring to Fig. 8A, with jaws 152, 154 in closed  
10 position, the biopsy jaws and ring electrode 168 are used to locate the region of the heart wall that is to be sampled (and possibly ablated). Differential electrical signals from the heart wall and the blood volume within the right ventricle are detected between the ring  
15 electrode and the biopsy jaws (or between the ring electrode and one or more additional ring electrodes, if present). These signals are delivered through electrical wire 170 and actuation wire 60 to a processor and to a display device for analysis.

Referring to Fig. 8B, when the location of the  
20 region of heart tissue to be sampled (ablated) is determined, the jaws are opened by moving the actuation knob distally (as indicated by arrow 64 in Fig. 1). With the jaws fully open, the catheter tip is deflected by  
25 pushing distally on thumbrest 108 (indicated by arrow 56 in Fig. 1), which presses the jaws against the myocardial tissue, increasing the normal force 128 applied by the electro-coagulation surfaces of the jaws. The deflection of the catheter tip is locked in place by twisting the  
30 piston relative to the handle housing. The operator then moves the actuation knob in the proximal direction to close the jaws about the selected portion of tissue and to cut the tissue. The cut tissue is retained within the cavity defined by the jaws during removal of the catheter  
35 from the patient's body.

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If the selected region of tissue is to be ablated, the operator moves the actuation knob in the proximal direction to partially close the jaws, thereby actively fixing (gripping) the catheter tip onto the tissue to be ablated. Rf energy is delivered through the actuation wire to the jaws until the desired amount of myocardial tissue is ablated (e.g., for a period of about 30 seconds to 1 minute). The combination of the fixation feature and the large surface area of the electrode sections exposed for contact with heart tissue enables deep, large area ablations to be achieved with a high degree of control.

We note the following co-pending applications, which are all herein incorporated by reference: Serial No. 08/138,863, filed October 19, 1993, U.S. Serial No. 08/038,903, filed March 29, 1993, and U.S. Serial No. 08/086,543, filed July 1, 1993, and U.S. Serial No. \_\_, filed February 28, 1995, to Klein et al., and entitled "Deflectable Catheter for Ablating Cardiac Tissue."

Still other embodiments are within the scope of the claims.

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What is claimed is:

1. A deflatable biopsy catheter for obtaining a tissue sample from a body cavity of a patient comprising an axially elongated catheter shaft having  
5 proximal and distal portions respectively terminating at proximal and distal ends, the catheter shaft being sized and constructed to be advanced into a body cavity of a patient,  
10 a deflection wire coupled to the distal portion of the catheter shaft and extending within the catheter to the proximal end thereof, and  
a pair of biopsy jaws coupled to the distal end of the catheter shaft and having first and second opposed free cutting surfaces exposable for contact with a  
15 selected area of tissue within the patient's body cavity and movable with respect to each other to cut a tissue sample from the selected area of tissue.
2. The deflatable biopsy catheter of claim 1 wherein the biopsy jaws are formed of hollow cup-shaped  
20 members that are pivotally hinged together about a pivot bearing coupled to the distal end of the catheter shaft.
3. The deflatable biopsy catheter of claim 1 further comprising an axially elongated actuation wire coupled to the biopsy jaws and extending proximally  
25 therefrom to the proximal end of the catheter shaft, the actuation wire being constructed and arranged to selectively move the jaws.
4. The deflatable biopsy catheter of claim 3 further comprising a tracking member coupled to the  
30 deflection wire and constructed and arranged to track movement of the actuation wire and to couple tension on the actuation wire to the deflection wire to counteract

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force applied by the actuation wire to the distal portion of the catheter during movement of the jaws.

5        5.     The deflatable biopsy catheter of claim 4 wherein the deflection wire and the actuation wire are arranged on radially opposed sides of the catheter axis in the distal portion of the catheter shaft.

10       6.     The deflatable biopsy catheter of claim 4 wherein the distal portion of the catheter shaft defined first and second no-coaxial lumens, the first and second lumens being radially offset from the axis of the catheter shaft, the deflection wire being disposed in the first radially offset lumen and the actuation wire being positioned in the second radially offset lumen.

15       7.     The deflatable biopsy catheter of claim 1 wherein the opposed jaws are formed from electrically conducting material and together form a generally dome-shaped outer electrically conducting surface.

20       8.     The deflatable biopsy catheter of claim 1 wherein cutting surfaces of the biopsy jaws exposable for contact with the selected area of heart tissue respectively comprise a plurality of serrated teeth for cutting body tissue.

25       9.     The deflatable biopsy catheter of claim 1 further comprising a needle coupled to the distal end of the catheter shaft and constructed and arranged to penetrate heart tissue to a selected depth.

      10.    The deflatable biopsy catheter of claim 1 wherein the biopsy jaws respectively include hollow cup-shaped distal sections for cutting tissue coupled to

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solid proximal sections having flat surfaces exposable for contact with tissue for ablation.

11. A method for obtaining a tissue sample from a body cavity of a patient comprising the steps of:

- 5       advancing a deflectable biopsy catheter, as defined in claim 1, within a body cavity of a patient; steering the catheter through the patient's body cavity and to a selected portion of body tissue by selectively deflecting the distal end of the catheter by  
10 applying tension to the deflection wire; opening the opposed jaws in the vicinity of the selected portion of body tissue; torquing the catheter shaft and deflecting the distal end of the catheter so that the opposed jaws are  
15 positioned about the selected portion of body tissue; and closing the jaws to cut a sample of tissue from the selected portion of body tissue.

12. The method of claim 11 wherein the opposed biopsy jaws together form an exposed electrically  
20 conductive surface, the method further comprising the step of

electro-coagulating the selected area of heart tissue by supplying to the electrically conductive surface formed by the biopsy jaws energy sufficient to  
25 achieve tissue electro-coagulation.

13. The method of claim 12 further comprising the step of deflecting a distal portion of the catheter to increase pressure applied by the exposed conductive surface of the biopsy jaws against the selected portion  
30 of tissue during electro-coagulation.

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14. A method for obtaining a tissue sample from the heart of a patient comprising the steps of:

advancing a deflectable biopsy catheter, as defined in claim 1, through the vasculature of a patient,  
5 wherein the opposed biopsy jaws together form an exposed electrically conductive electrode surface and further comprising a second electrically conductive electrode surface;

steering the catheter through the vasculature and  
10 into the heart of the patient by deflecting the distal end of the catheter by applying tension to the deflection wire;

selecting the area of heart tissue to be diagnosed based on measurements of electrical potentials within the  
15 patient's heart between the first and second electrode surfaces;

opening the opposed jaws in the vicinity a selected portion of heart tissue;

torquing the catheter shaft and deflecting the  
20 distal end of the catheter so that the opposed jaws are positioned about the selected portion of heart tissue; and

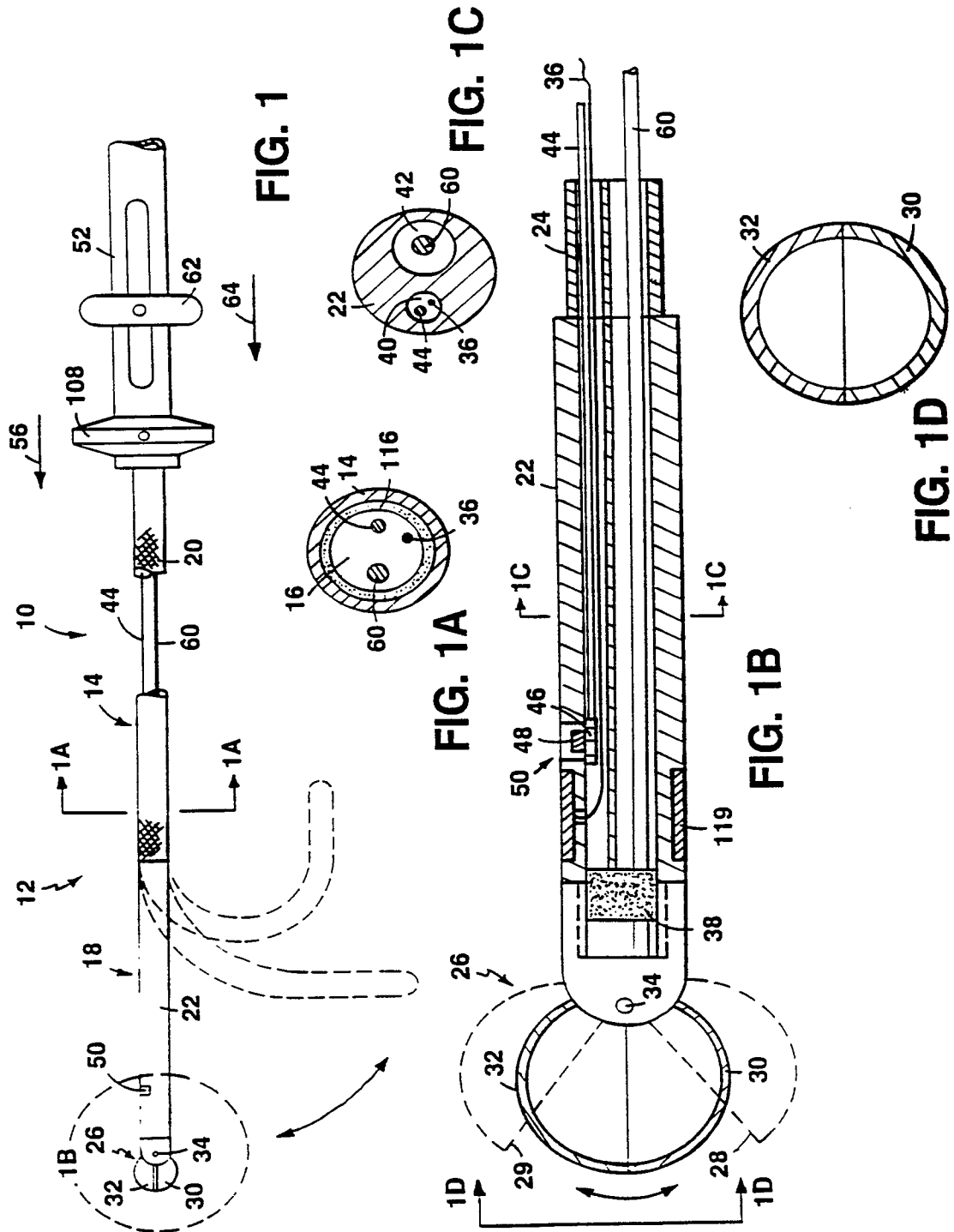
closing the jaws to cut a sample of tissue from the selected portion of heart tissue.

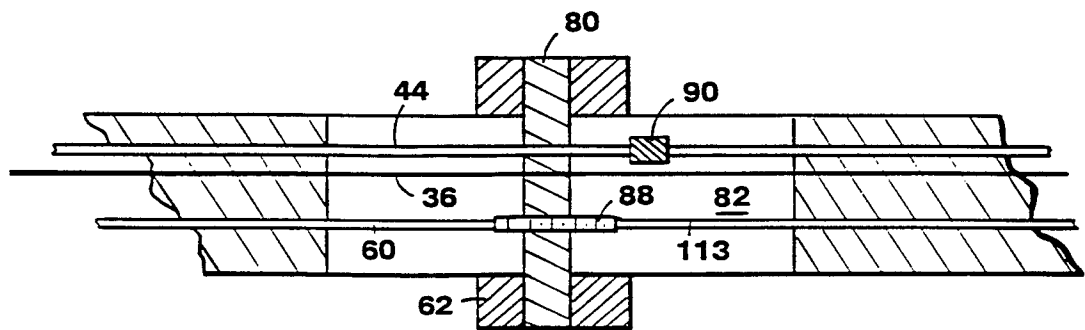
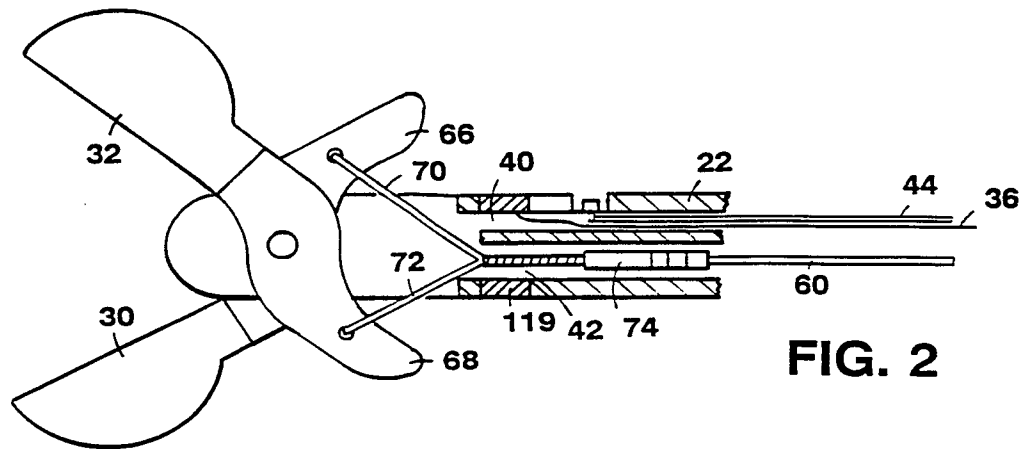
25 15. The method of claim 14 further comprising the steps of

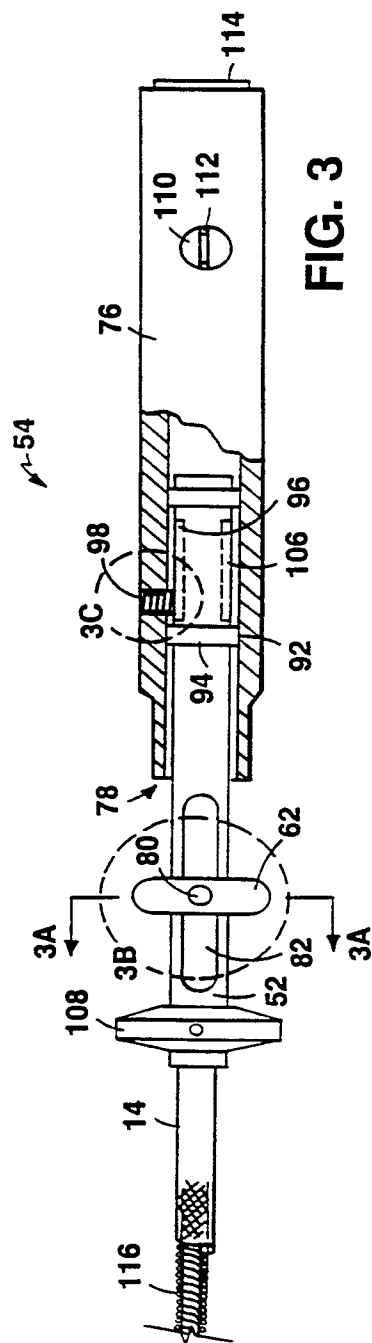
selecting an area of heart tissue to be ablated based on measurements of electrical potentials within the heart between the first and second electrode surfaces,  
30 and

ablating the are of heart tissue selected to be ablated by supplying to the electrically conductive surface formed by the biopsy jaws energy sufficient to achieve tissue ablation.

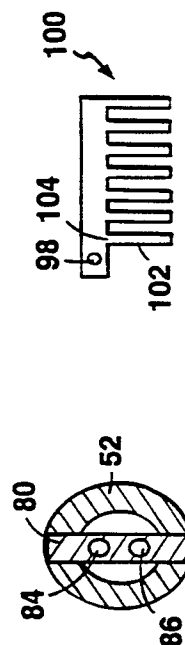




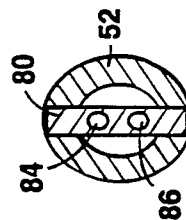




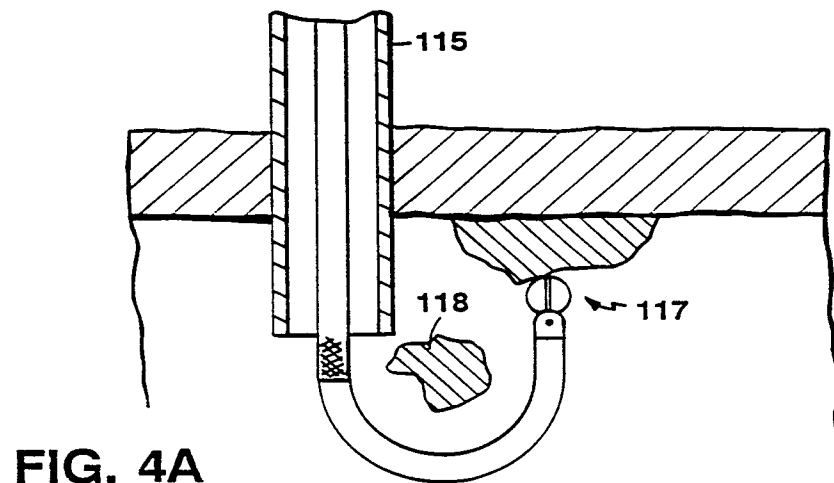
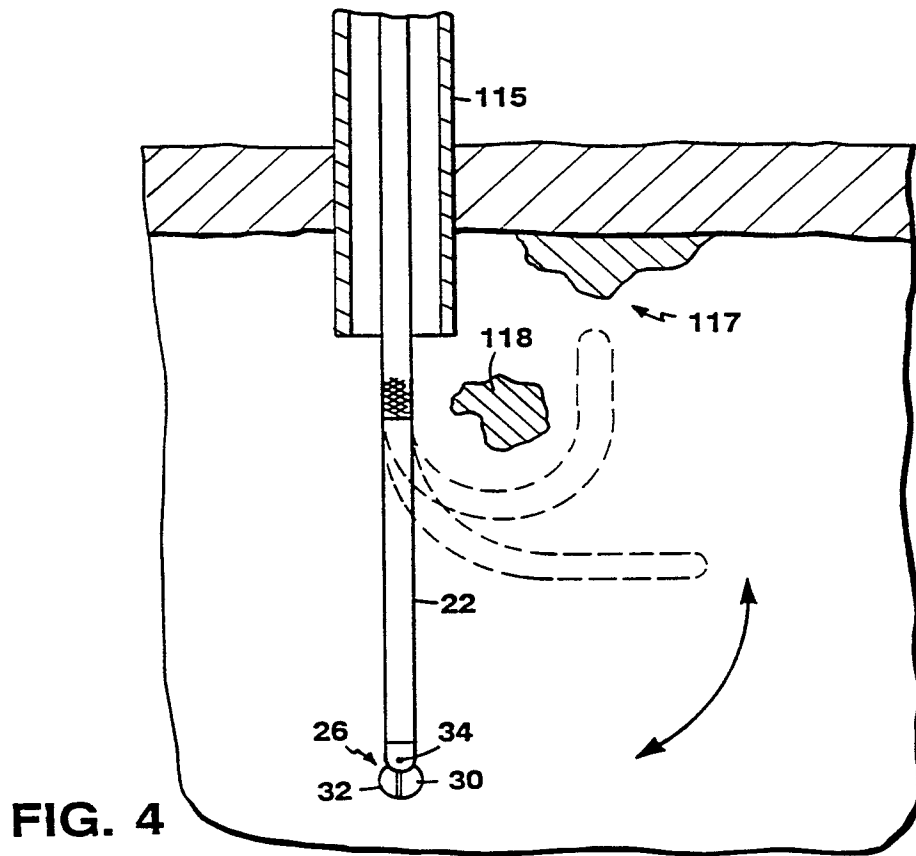
**FIG. 3**

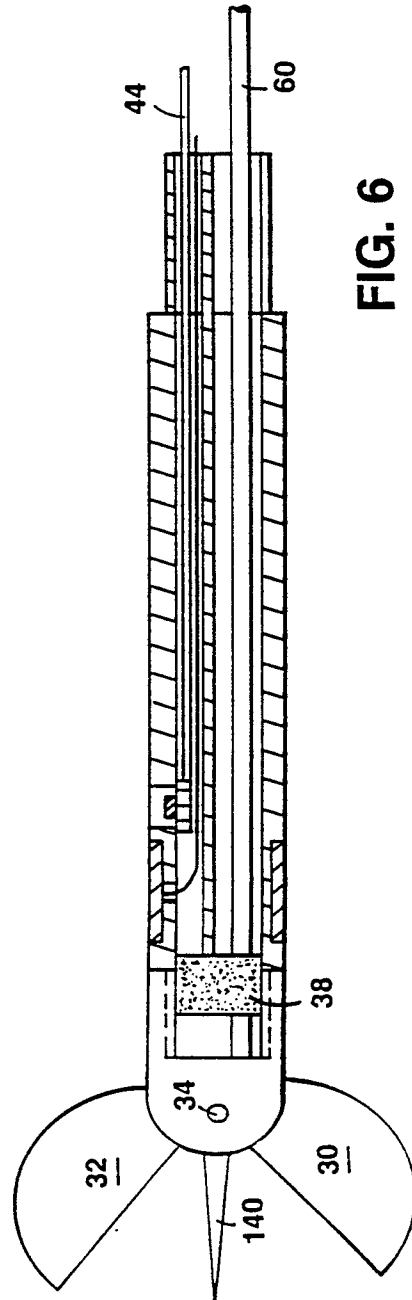
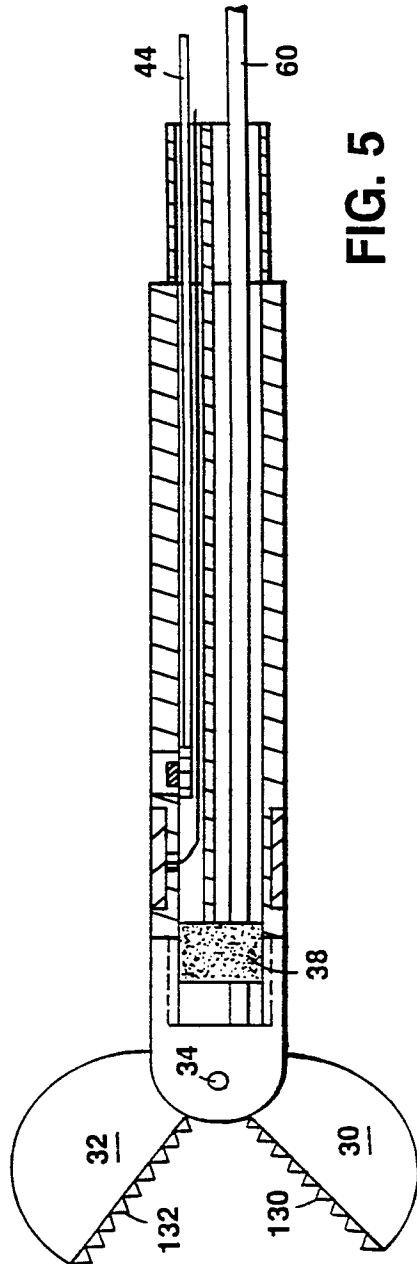


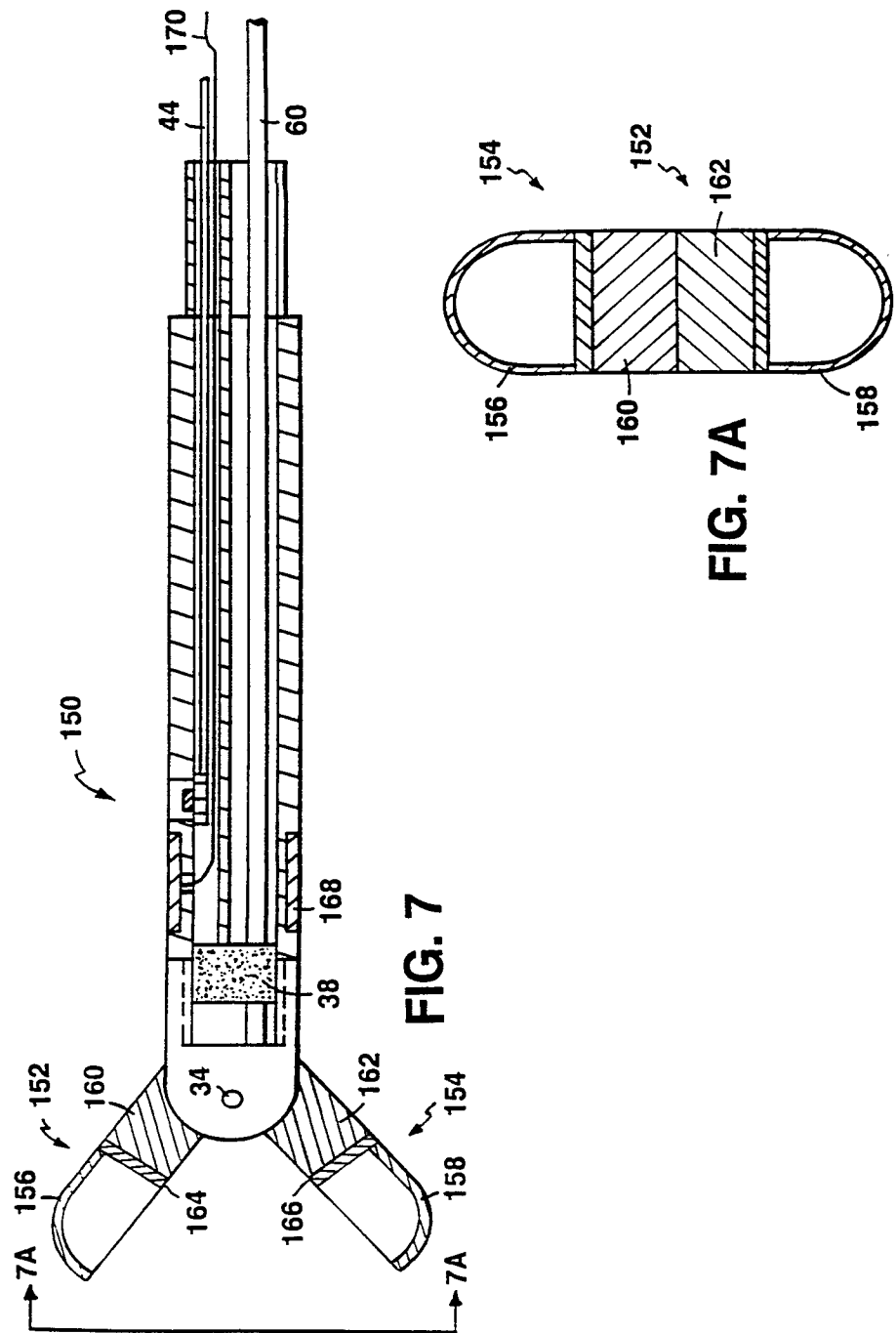
**FIG. 3C**

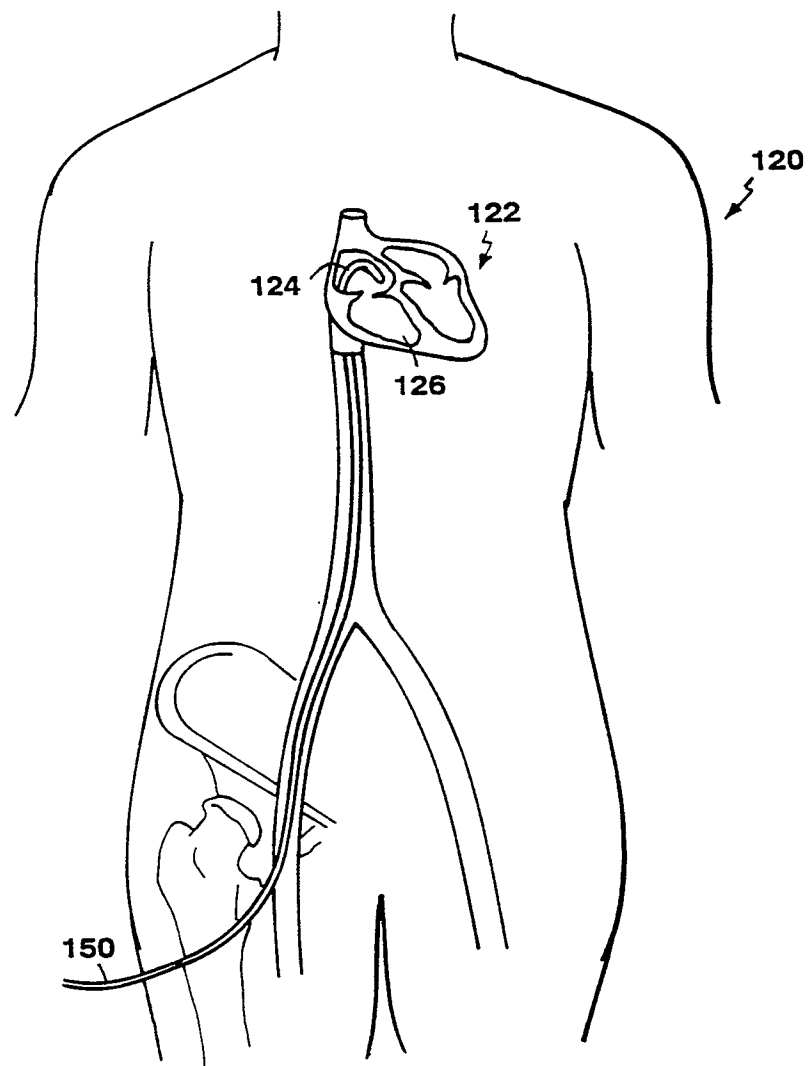


**FIG. 3A**







**FIG. 8**

