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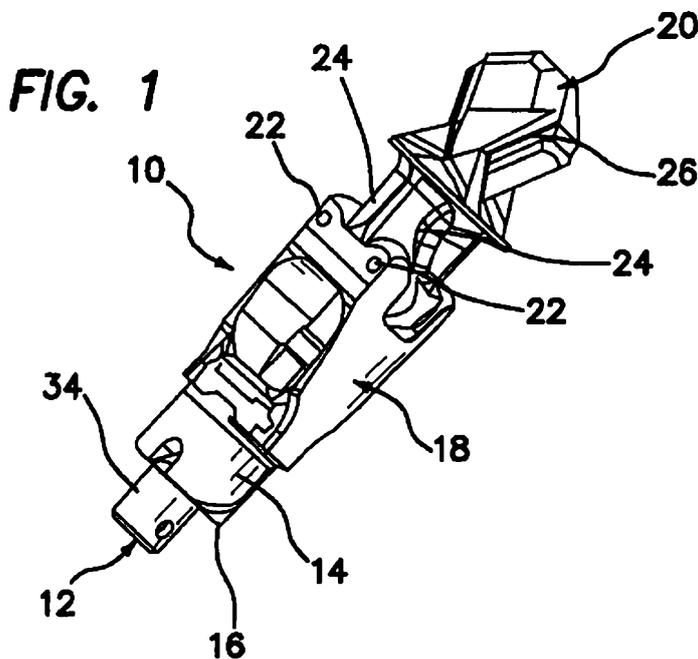
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(57) Abstract: A soft tissue fixation system, most typically applicable to orthopedic joint repairs, such as anterior cruciate ligament (ACL) knee repair procedures, comprises an implant which is placeable in a tunnel disposed in a portion of bone, wherein the tunnel is defined by walls comprised of bone. A first member is deployable outwardly to engage the tunnel walls for anchoring the implant in place in the tunnel, and a second member is deployable outwardly to engage tissue material to be fixed within the tunnel. The second member also functions to move the tissue material outwardly into contact with the tunnel walls to promote tendon-bone fixation. Extra graft length is eliminated by compression of the tendon against the bone at the aperture of the femoral tunnel, which more closely replicates the native ACL and increases graft stiffness.

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METHODS AND SYSTEMS FOR MATERIAL FIXATION

Background of the Invention

The present invention relates generally to devices, systems and methods for material fixation. More specifically, the present invention relates to a
5 technique that can be used to firmly hold a soft tissue or graft against bone tissue within a bone tunnel.

One of the most common needs in orthopedic surgery is the fixation of tendon to bone. The fixation of diseased tendons into a modified position is called tenodesis and is commonly required in patients with injury to the long
10 head of the biceps tendon in the shoulder. In addition, tendons which are torn from their insertion site into bone also frequently require repair. This includes distal biceps tendon tears, rotator cuff tears, and torn flexor tendons in the hand. Tendons are also frequently used in the reconstruction of unstable joints. Common examples include anterior cruciate ligament and collateral ligament
15 reconstructions of the knee, medial and lateral elbow collateral ligament reconstructions, ankle collateral ligament reconstruction, finger and hand collateral ligament reconstructions and the like.

Traditional techniques that are used to fix tendon to bone suffer from a number of limitations as a result of the methodology used, including the use of a
20 "keyhole" tenodesis, pull-out sutures, bone tunnels, and interference screw fixation. The "keyhole" tenodesis requires the creation of a bone tunnel in the shape of a keyhole, which allows a knotted tendon to be inserted into the upper portion, and subsequently wedged into the lower narrower portion of the tunnel where inherent traction on the tendon holds it in place. This technique is
25 challenging as it is often difficult to sculpt the keyhole site and insert the tendon into the tunnel. In addition, if the tendon knot unravels in the postoperative period, the tendon will slide out of the keyhole, losing fixation.

Another traditional form of tendon fixation is the use of the “pull-out stitch.” With this technique, sutures attached to the tendon end are passed through bone tunnels and tied over a post or button on the opposite side of the joint. This technique has lost favor in recent years due to a host of associated complications, which include wound problems, weak fixation strength, and potential injury to adjacent structures.

The most common method of fixation of tendon to bone is the use of bone tunnels with either suture fixation, or interference screw fixation. The creation of bone tunnels is relatively complicated, often requiring an extensive exposure to identify the margins of the tunnels. Drill holes placed at right angles are connected using small curettes. This tedious process is time-consuming and fraught with complications, which include poor tunnel placement and fracture of the overlying bone bridge. Graft isometry, which is easy to determine with single point fixation, is difficult to achieve because the tendon exits the bone from two points. After creation of tunnels, sutures must be passed through the tunnels to facilitate the passage of the tendon graft. Tunnels should be small enough to allow good tendon-bone contact, yet large enough to allow for graft passage without compromising the tendon. This portion of the procedure is often time-consuming and frustrating to a surgeon. Finally, the procedure can be compromised if the bone bridge above the tunnel breaks, resulting in loss of fixation. The technique restricts fixation to the strength of the sutures, and does not provide any direct tendon to bone compression.

More recent advances in the field of tendon fixation involve the use of an internally deployed toggle button, for example, the EndoButton[®], and the use of interference screws to provide fixation. The EndoButton, by Smith & Nephew, allows the fixation of tendon into a bone tunnel by creating an internally deployed post against a bony wall. While this technique eliminates the need for secondary incisions to place the post, the fixation strength is limited to suture strength alone. This technique does not provide direct tendon to bone compression; as such this technique may slow healing and lead to graft tunnel

widening due to the “bungee effect” and “windshield wiper effect”. As a result, this technique has limited clinical applications and is used primarily for salvage when bone tunnels break or backup fixation is important.

The use of the interference screw is the most notable advance in the
5 fixation of tendon to bone. The screw is inserted adjacent to a tendon in a bone tunnel, providing axial compression between the screw threads and the bony wall. Advantages include acceptable pull-out strength and relative ease of use. Aperture fixation, the ability to fix the tendon to bone at its entrance site, is a valuable adjunct to this technique as it minimizes graft motion and subsequent
10 tunnel widening. Some disadvantages related to soft tissue interference screws are that they can be difficult to use, and can also cut or compromise the tendon during implantation.

The newest generation interference screw allows the ability to provide tendon to bone fixation with limited exposure. For example, the Bio-Tenodesis
15 Screw™ (Arthrex, Inc.) allows the tensioning and insertion of tendon into bone, followed by insertion of an adjacent soft tissue interference screw. While this screw system provides advantages in the insertion of tendon into bone in cases when a pull through stitch is not available, it is still limited by the potential for tendon rotation or disruption as the screw compresses the tendon. The surgical
20 technique is also complicated, typically requiring two or more hands for insertion, making it difficult to use the system without assistance during arthroscopic or open procedures. Finally, the use of the screw requires preparation of the tendon end, which can be difficult, time consuming, and can also require conversion of an arthroscopic procedure to open.

25 Referring particularly to the field of repairing an anterior cruciate ligament (ACL) injury, current repair techniques utilizing soft tissue for the replacement graft are either difficult to perform or they result in less than favorable outcomes due to their relatively low tendon-to-bone fixation. Existing ACL reconstruction techniques that have acceptable outcomes (high tendon-to-
30 bone fixation strength) require extra operating room time and surgeon effort due to the requirements of multiple drill holes, external guides and fixtures for the

drill holes, and multiple assistants. Another difficulty with current techniques is that they do not well replicate the native ACL in its anatomy or physiology.

Two important factors in replicating the native ACL are aperture compression (compressing the tendon against the bone at the opening of the drill hole into the joint) and tendon length. Compression of the tendons at the aperture of the femoral tunnel will improve the healing process by increasing the intimate contact between the tendon and the bone. Studies show that the lack of intimate contact between the tendon and bone can result in less well organized fibrous tissue, resulting in lower pull-out strengths. The stiffness of the repair is also important to replicate the native ACL. Graft stiffness is decreased by the length of tendon between the fixation points.

Currently, two different sources are utilized for the tissue that replaces the injured native ACL. When the new tissue comes from the patient's own body, the new graft is referred to as an autograft, and when cadaveric tissue is used, the new graft is referred to as an allograft. The most common autograft ACL reconstruction performed currently is the bone-patellar tendon-bone (BTB) graft. The BTB graft fixed with an interference screw is used more often because it more accurately replicates the native ACL, due to its aperture compression at the femoral tunnel aperture. However, BTB reconstructions result in an increased rate of anterior knee pain post-surgically for periods of up to 3 years after the reconstruction. Additionally, the harvest procedure for the BTB autograft is invasive and can be difficult to perform. Alternatively, the hamstring tendon autograft ACL reconstruction technique does not result in any significant post-surgical pain, and the harvest procedure is minimally invasive compared to the BTB graft harvest. The reason that the hamstring tendon autograft procedure is not used more frequently in ACL reconstructions is that the fixation of the hamstring tendons to the femur and tibia are not as strong as the fixation of the BTB autografts.

Many prior art systems have addressed some of the problems associated with ACL reconstruction using hamstring tendons, but there is not one system that addresses them all. For example, the EndoButton system (Smith &

Nephew) is easy to use and does not need additional drill holes. However, it does require additional accessories and additional people to perform the procedure and does not replicate the native ACL due to a lack of tendon-to-bone compression at the aperture, as well as additional length of tendon between
5 fixation points. The EndoButton system is an example of a cortical hamstring fixation device that yields a longer graft construct, resulting in a graft that is less stiff than the native ACL. Peer reviewed journal data show that existing soft tissue fixation systems with long graft lengths between fixation points have as much as a 56% reduction in graft stiffness when compared to the native ACL.

10 The RigidFix[®] product by Mitek is a cross pin device that requires multiple drill holes, additional instruments, and assistance from other people in the operating room to complete the repair. Also, there is only passive compression of tendon to bone, not direct, active compression.

The Stratis[®] ST product by Scandius attempts to more accurately
15 replicate the native ACL by adding material to take up space in the femoral tunnel resulting in more intimate contact between the tendon and the bone. However, to insert the device into the femoral tunnel, the cross-sectional area must be less than the cross-sectional area of the hole. Thus, there is no real compression of tendon to bone. The Stratis ST product also requires additional
20 drill holes, accessories, and people to properly perform the procedure.

The EZLOC[™] product by Arthrotek provides high strength and attempts to more accurately replicate the native ACL in the same fashion as the Stratis ST product, by taking up the space in the femoral tunnel. This does create more intimate contact between the tendon and bone, but does not offer real
25 compression at the aperture.

Interference screws such as the RCI[™] Screw, available from Smith & Nephew, are easy to use and provide compression of tendon to bone at the femoral tunnel aperture. However, the pull-out strength and stiffness of the repair are significantly lower than the preceding systems.

30 Thus, although there are many conventional techniques used for the fixation of tendon to bone, each having some advantages, the disadvantages of

each such technique presents a need in the art for a simple and universal technique to fixate tendon to bone such that the device is easy to use, the process is simple to follow, and the result is a firm and secure tendon to bone fixation with minimal negative effect on the tendon. Further, such device should be easy to manufacture, universally applied to different tendon to bone sites, and require minimal effort to understand and use in practice.

OBJECT OF THE INVENTION

It is the object of the present invention to substantially overcome or ameliorate one or more of the above disadvantages, or at least provide a useful alternative.

SUMMARY OF THE INVENTION

In one aspect, the present invention provides a material fixation system, comprising:
an implant comprising a body having a distal end and a proximal end which is placeable in a tunnel disposed in a portion of bone, wherein the tunnel is defined by walls comprised of bone;

a first member which is deployable outwardly to engage adjacent bone for anchoring said implant in place in the tunnel;

a second member which is deployable outwardly to engage tissue material to be fixed within said tunnel, and to move the tissue material outwardly into contact with the tunnel walls, wherein said second member comprises blunt tissue engaging surfaces which engage the tissue without piercing it; and

a third member which is movable generally axially to deploy said first member outwardly.

In another aspect, the present invention provides an implant system for use in making an orthopedic repair of a joint, said implant system comprising:

a first implant adapted for receiving a tissue graft thereon and then being disposed in a first bone tunnel location, wherein ends of the tissue graft extend through a bone tunnel and out of a proximal end of the tunnel, said first implant comprising:

a body portion having a distal end and a proximal end;

a first member disposed on said body portion which is deployable outwardly to engage adjacent bone for anchoring said implant place in the tunnel;

a second member disposed on said body portion which comprises blunt surfaces that are deployable outwardly to engage tissue material to be fixed within said tunnel,

and to move the tissue material outwardly into contact with the tunnel walls without piercing the tissue or the tunnel walls;

a third member comprising a wedge which is movable generally axially to deploy said first member outwardly; and

a fourth member for actuating said third member to move in order to deploy said first member; and

a second implant adapted for disposition in a second bone tunnel location, proximal to said first bone tunnel location, said second implant being adapted to secure the ends of the tissue graft which extend from the first implant against adjacent bone.

There is also disclosed herein an anchor for securing soft tissue into a portion of bone, comprising:

a body portion having a distal end and a proximal end;
at least one outwardly deployable anchoring member disposed on said body;
a wedge member which is movable for deploying said at least one outwardly deployable anchoring member; and
a generally axially movable deploying member for moving said wedge member.

Other preferred aspects and preferred embodiments will now be described.

The preferred embodiment provides a device that is easy to use, provides high fixation of tendon-bone and active tendon-bone compression, requires no additional accessories, uses only one drill hole, and can be implanted by one practitioner. The preferred embodiment utilizes cancellous bone for fixation, and replicates the native ACL by compressing the tendons against the bone at the aperture of the femoral tunnel, effectively shortening the length of the graft as compared to cortical hamstring fixation devices. An important advantage of the preferred embodiment is the improvement of the tendon-bone fixation of hamstring autografts as well as other soft-tissue ACL reconstruction techniques. Extra graft length is eliminated by compression of the tendon against the bone at the aperture of the femoral tunnel, which more closely replicates the native ACL and increases graft stiffness. The inventive device provides high fixation of tendon to bone and active tendon-bone compression. Graft strength has been found to be greater than 1,000 N (Newtons), which is desirable for ACL reconstruction systems.

More particularly, there is provided a material fixation system, which comprises an implant which is placeable in a tunnel disposed in a portion of bone, wherein the tunnel is defined by walls comprised of bone. A first member is deployable outwardly to engage the tunnel walls for anchoring the implant in place in the tunnel, and a second member is deployable outwardly to engage tissue material to be fixed within the tunnel. The second member also functions to move the tissue material outwardly into contact with the tunnel walls. A third member forming a part of the implant is movable to deploy the first member outwardly. A fourth member is provided actuating the third member to move in order to deploy the first member.

Preferably, the fourth member comprises a portion which functions to deploy the second member outwardly. The implant comprises a body having a distal end and a proximal end, and the first member is disposed on the body. The first member comprises an arm which is pivotally attached to the body. The third member comprises a wedge which is movable generally axially to deploy the arm.

In one presently preferred embodiment, the fourth member comprises a deployment screw having a distal end and a proximal end, wherein the deployment screw is adapted to extend axially through the body. The distal end of the deployment screw has a threaded portion which is engageable with a complementary threaded portion on the wedge, wherein rotation of the deployment screw causes relative movement of the deployment screw and the wedge. The wedge moves proximally to deploy the arm.

The aforementioned second member comprises a compression pad. In the preferred embodiment, the fourth member portion comprises a head of the deployment screw, disposed on the proximal end thereof.

There is also disclosed herein an anchor for securing soft tissue into a portion of bone, which comprises a body portion having a distal end and a proximal end. At least one outwardly deployable anchoring member is disposed on the body. A wedge member is movable for deploying the at least one outwardly deployable anchoring member. The anchor further comprises a generally axially movable deploying member for moving the wedge member. The deploying member engages the wedge member to move the wedge member, and is disposed proximally of the wedge member.

Preferably, the aforementioned wedge member is disposed distally of the outwardly deployable anchoring member, and moves proximally in order to deploy the outwardly deployable anchoring member outwardly. The anchor further comprises an outwardly deployable compression member for engaging a portion of soft tissue and pushing the soft tissue outwardly into contact with adjacent bone. The outwardly deployable compression member is proximal to the outwardly deployable anchoring member. A portion of the generally axially movable deploying member is adapted to deploy the compression member outwardly. Again, referencing currently preferred embodiments, the at least one outwardly deployable anchoring member comprises an arm pivotally attached to the body, and the generally axially deploying member comprises a threaded deployment screw.

There is also disclosed herein an implant system for use in making an orthopedic repair of a joint, which comprises a first implant adapted for receiving a tissue graft thereon and then being disposed in a first bone tunnel location, wherein ends of the tissue graft extend through a bone tunnel and out of a proximal end of the tunnel. The first implant comprises a body portion having a distal end and a proximal end, and a first member disposed on the body portion which is deployable outwardly to engage adjacent bone for anchoring the implant in place in the tunnel. The first implant further comprises a second member disposed on the body portion which is deployable outwardly to engage tissue material to be fixed within the tunnel, and to move the tissue material outwardly into contact with the tunnel walls. The implant system further comprises a second implant adapted for disposition in a second bone tunnel location, proximal to the first bone tunnel location. The second implant is adapted to secure the ends of the tissue graft which extend from the first implant against adjacent bone. The first implant further comprises a third member which is movable to deploy the first member outwardly. A fourth member is provided for actuating the third member to move in order to deploy the first member.

There is also disclosed herein a method of making an orthopedic repair by fixing a soft tissue graft to bone, which comprises steps of placing a soft tissue graft on an implant, and disposing the implant within a bone tunnel at a desired location, such that a plurality of ends of the soft tissue graft extend from the implant in a proximal direction through the bone tunnel. Additional steps include deploying a first member on a body of the implant outwardly so that portions of the first member engage adjacent bone to secure the implant in place at the desired location, and deploying a second member on the body of the implant outwardly, so that portions

of the second member engage portions of the plurality of ends of the soft tissue graft and push the soft tissue graft ends into contact with adjacent bone.

BRIEF DESCRIPTION OF THE DRAWINGS

Preferred embodiments of the invention will be described hereinafter, by way of example only, with reference to the accompanying drawings, wherein:

Fig. 1 is an isometric view of an embodiment of a device constructed in accordance with the principles of the present invention;

Fig. 2A is a top view of the device of Fig. 1 in an undeployed configuration;

Fig. 2B is a side view of the device of Fig. 2A;

Fig. 3A is a top view of the device of Fig. 1, wherein the deployment screw is starting to deploy the compression pads;

Fig. 3B is a side view of the device of Fig. 3A;

Fig. 4A is a top view of the device of Fig. 1, wherein the compression pads have been fully deployed;

Fig. 4B is a side view of the device of Fig. 4A;

Fig. 5 is a top view of the device of Fig. 1, wherein the wedge is starting to deploy the arms;

Fig. 6 is a top view of the device of Fig. 1, wherein the wedge is halfway engaged;

5 Fig. 7A is a top view of the device of Fig. 1, wherein the implant has been fully deployed;

Fig. 7B is a side view of the device of Fig. 7A;

Fig. 8 is a view illustrating the implant of Fig. 1, as it is deployed in the femoral tunnel of a patient;

10 Fig. 9A is a view illustrating tendon compression as effected by the embodiment of Figs. 1-7;

Fig. 9B is a detail view of a portion of Fig. 9A denoted by a circle labeled as "9B";

Fig. 10 is a perspective view, in isolation, of a deployment screw for use
15 in the embodiment of Figs. 1-7;

Fig. 11A is a perspective view of a compression pad for use in the embodiment of Figs. 1-7;

Fig. 11B is a perspective view of a second compression pad;

Fig. 12 is a perspective view of the body of the implant of Figs. 1-7;

Figs. 13A and 13B are perspective views of arms for use in the embodiment of Figs. 1-7;

Figs. 14A and 14B are perspective views of the wedge for use in the embodiment of Figs. 1-7;

5 Figs. 15A and 15B are perspective views of modified embodiments of the implant of Figs. 1-7 with arms flipped to engage with the cortical surface during a soft tissue repair procedure;

Figs. 16A and 16B are perspective views of yet another embodiment of the implant of the invention, wherein the body is used as the wedge;

10 Fig. 17 is a table summarizing the performance of an implant constructed in accordance with the principles of the present invention, as shown in Figs. 1-7;

Fig. 18 is an isometric view of a further modified embodiment of the invention;

Fig. 19 is an exploded view of the embodiment of Fig. 18;

15 Fig. 20 is a plan view of the embodiment of Fig. 18, in an undeployed configuration;

Fig. 21 is a side view of the embodiment of Fig. 20;

Fig. 22 is a plan view of the embodiment of Fig. 20, wherein the deployment screw is starting to deploy the compression pads;

20 Fig. 23 is a side view of the embodiment of Fig. 22;

Fig. 24 is a view illustrating the implant of Figs. 18-23 deployed in a femoral tunnel;

Fig. 25 is a detailed view similar to Fig. 24, showing tendon compression performed by the deployed inventive device;

5 Fig. 26 is a perspective view of the deployment screw;

Fig. 27 is a view showing the body of the implant;

Fig. 28 is a view similar to Fig. 27, but showing the implant from a different orientation;

Fig. 29 is an isometric view of an arm in accordance with the invention;

10 Fig. 30 is an isometric view from a different orientation than Fig. 29, showing the arm;

Fig. 31 is a view of the wedge of the invention;

Fig. 32 is a data table;

15 Fig. 33 is an isometric view of another embodiment of the invention, comprising an undeployed cortical fixation implant;

Fig. 34 is an isometric view of the cortical fixation implant of Fig. 33, from a different orientation;

Figs. 35 and 36 are top and side views, respectively, of the cortical implant of Figs. 33 and 34;

Figs. 37 and 38 are top and side views, respectively, of the cortical implant of Figs. 33 and 34, wherein the implant is beginning to be deployed;

Figs. 39 and 40 are top and side views, respectively, of the cortical implant of Figs. 37 and 38, wherein the implant is in a deployed state;

5 Figs. 41 and 42 show a deployment sequence for the cortical fixation implant;

Fig. 43 is an isometric view of the body of the implant of Fig. 33, showing integrated compression pads;

10 Fig. 44 is a cross-sectional view of the body of Fig. 43, taken along the lines 44-44 of Fig. 45;

Fig. 45 is a side view of the implant of Fig. 43;

Fig. 46 is a perspective view of the wedge of the invention;

Figs. 47 and 48 are views of the arm of the invention;

15 Fig. 49 is a perspective view of the compression wedge of the invention;

Fig. 50 is a perspective view of the deployment screw of yet another embodiment of the inventive implant; and

20 Figs. 51-52 are isometric views of an additional embodiment of a cortical implant of the invention, wherein Fig. 51 shows the device in its undeployed configuration and Fig. 52 shows the device in its deployed configuration;

Figs. 53-54 are isometric views of still another embodiment of a cortical implant of the invention, wherein Fig. 53 shows the device in its undeployed configuration and Fig. 54 shows the device in its deployed configuration; and

Fig. 55 is a view of the femur and tibia of a patient's leg, showing a
5 substantially completed ACL repair.

Detailed Description of the Invention

Referring now more particularly to the drawings, procedures and anchoring devices for repairing soft tissue are illustrated. In Fig. 1, one embodiment of an implant 10, constructed in accordance with the principles of
10 the present invention, is shown. The implant 10 comprises a deployment screw 12, which protrudes through a pair of compression pads 14 and 16. The implant 10 comprises a body 18, through which the deployment screw 12 also protrudes. The deployment screw 12, at its distal end, is threaded into a wedge 20.

The left compression pad 14 slides into the right compression pad 16,
15 and they attach to one another. Two pins 22 attach a pair of arms 24 to the body 18. There is a track 26 on each side of the wedge 20, best seen in Fig. 14A. Each wedge track 26 attaches to a track post 28 (Fig. 13B) on a corresponding one of the arms 24. The wedge tracks 26 function to prevent the wedge from rotating during deployment of the implant.

20 The compression pads 14, 16 slide into a pair of body tracks 30 (Fig. 12) in the body 18, which allow the pads 14, 16 to expand when the deployment screw 12 is rotated clockwise, as shown in Figs. 2-4. The body tracks 30 also prevent the pads 14, 16 from rotating.

In Fig. 10, the deployment screw 12 is shown in detail. This screw 12
25 comprises a quad lead section 32, with four separate thread starts. This means that, for every single turn on the screw, the linear distance it travels is four times what a single lead screw would be. This feature enables the user to turn the screw fewer times than would be required with a single start thread,

approximating the same number of turns that the user would need during the implantation of an interference screw such as the above described Smith & Nephew RCI screw. Often, during implantation, an interference screw requires a notch to be placed at the edge of the femoral tunnel aperture to allow the screw to start engaging into the bone. Advantageously, the need for this step is eliminated when deploying the implant of the present invention, resulting in a substantially easier implementation procedure.

Accordingly, the present invention is easy to deploy as an interference screw, and requires fewer steps than in prior art approaches. The deployment screw 12 also provides a rigid backbone to support the implant. A screw head or compression pad deployer 34 deploys the compression pads 14, 16 as the screw 12 moves axially into the implant. Another feature of the screw 12 is a load transfer disk 36 that transfers some of the axial load from a junction between the screw head 34 and the body 18 to a junction between the load transfer disk 36 and the body 18. This load transferring feature allows for thinner side walls or struts 38 on the body 18 due to a decreased load on struts 38 (Fig. 12), which, in turn, allows a larger tendon to fit between the deployment screw 12 and the body 18.

With reference now particularly to Figs. 11A and 11B, the compression pads 14 and 16 are shown in greater detail. The left and right compression pads 14, 16, respectively, compress the tendons against the femoral tunnel wall to promote tendon-to-bone healing at the aperture of the tunnel. Unlike current approaches for more intimate tendon-to-bone contact that only reduce the space between the tendon and the tunnel wall, the present invention actively compresses the tendons against the bone tunnel. Compression pad tracks 40 engage the body tracks 30 and interlock them to the body 18. This joint also provides torsional resistance while moving the implant into place, and during initial deployment until the arms 24 start to engage with the bone. There are engagement slots 42 in each compression pad 14, 16, as shown, that engage with a deployment device that keep the implant 10 from rotating until the arms

24 engage the bone. The two compression pads 14, 16 snap together using compression pad snaps 44 to prevent premature deployment of the pads.

Now referring to Fig. 12, the body 18 functions to trap the tendons on either side of the deployment screw 12. The compression pads 14, 16 engage
5 the body tracks 30 and provide torsional strength to the body while inserting the implant into the femoral tunnel, thus allowing the compression pads 14, 16 to expand parallel to one another. The struts 38 also provide structural support for the deployment screw 12, wedge 20, and arms 24 to deploy against.

The arms 24 have a few key design features, as best shown in Figs. 13A
10 and 13B. Fins 46 on the top of each arm provide torsional strength for the wedge-to-arm junction. The fins 46 also allow easier insertion into the femoral tunnel when inserting into a femoral tunnel that is drilled off-axis from the tibial tunnel. The portion of the arm 24 that engages with the bone has a tapered edge 48 which allows for ease of bone displacement during deployment. A support
15 rib 50 disposed along the length of the arm 24 is also tapered for ease of bone displacement, and provides structural support during axial loading. Torsion pins 52 engage with a torsion hole 54 to provide additional torsional strength while the implant is being implanted into the femoral tunnel.

Figs. 14A and 14B show, in greater detail, particular constructional
20 features of the wedge 20. The wedge 20 is threaded with a female quad lead thread 56 that matches the male quad lead thread 32 of the deployment screw 12. The track posts 28 engage with the wedge tracks 26 to provide torsional strength through deployment. A tapered nose 58 on the wedge 20 allows easier off-axis insertion into the femoral tunnel.

25 Referring now to Figs. 2-9, a preferred method of using the disclosed inventive implant will now be discussed. In Figs. 2A and 2B, the implant 10 of Fig. 1 is shown in its undeployed orientation. A preferred procedure for deploying the implant is generally similar in many respects to the procedure disclosed in U.S. Patent Application Publication No. 2006/0155287, herein
30 already expressly incorporated by reference.

Thus, to accomplish tendon fixation using the exemplary methods and devices described herein, standard surgical preparation of the site and/or arthroscopic portals for access to the procedural region are performed. The joint is dilated with arthroscopic fluid if the procedure is to be performed
5 arthroscopically. With open procedures, the device may easily be manipulated and deployed with a single hand. For arthroscopic procedures, the deployment device is introduced through a standard 5, 6, or 8 mm cannula placed into the joint. A range of preferred cannula sizes would be 2-11 mm.

The procedures described herein are specifically adapted to repair of the
10 ACL in a patient's knee. However, it should be kept in mind that the implants described herein may be used in numerous other soft tissue repair applications, using surgical procedures which are adapted to those applications.

Figs. 8 and 9A illustrate, from two different orientations, a hamstring ACL reconstruction, wherein the implant 10 is utilized to secure the ACL graft
15 proximal to the femur 60 and distal to the tibia 62 of a patient. To deploy the implant 10, a bone tunnel 64 is drilled completely through the tibia 62 and partially through the femur 60. An actuator (not shown) is employed to insert the implant 10 distally through a tibial inlet aperture 66 and through the tibial tunnel 64, so that the implant 10 is finally disposed in a portion of the tunnel 64
20 which is within the femur 60, distal to a femoral aperture 68, as shown in Figs. 8 and 9A.

Now with respect to Figs. 3 and 3A, once the implant 10 is in place within the femoral tunnel 64, as shown in Fig. 8, the deployment screw 12 is actuated (rotated) in order to advance the screw 12 axially distally into the
25 implant body 18, and thus begin to deploy or expand the compression pads 14 and 16 outwardly. Figs. 4 and 4A depict the next step, wherein advancement of the deployment screw 12 has caused the compression pads 14, 16 to fully deploy. As noted above, the screw head or compression pad deployer 34 acts to deploy the compression pads 14, 16 as it moves distally into the implant 10, as
30 shown.

As the deployment screw 12 continues to move distally through the implant 10, the distal end of the screw 12, comprising the male quad lead section 32 (Fig. 10), engages the female quad lead thread 56 of the wedge 20 (Fig. 14B). Continued axial distal movement of the screw 12 causes the threaded sections 32 and 56 to cooperate to move the wedge 20 axially in a proximal direction, as shown in Fig. 5. This proximal movement of the wedge 20 causes the arms 24 to begin to deploy outwardly. In Fig. 6, the wedge 20 is shown in a position where it is about halfway engaged within the separating arms 24.

10 In Figs. 7A and 7B, the wedge 20 is fully proximally engaged with the body 12 of the implant 10, such that the arms 24 are, consequently, fully deployed. In Fig. 8, the implant 10 is shown in this fully deployed condition.

Figs. 9A and 9B illustrate tendon compression as effected by the deployed implant 10. In these figures, tendons 70 are compressed by deployed compression pads 14, 16 against the femoral tunnel wall in order to promote tendon-to-bone healing at the aperture of the tunnel. Advantageously, the inventive approach actively compresses the tendons against the bone tunnel.

Alternative implant designs are shown in Figs. 15 and 16. In particular, Figs. 15A and 15B illustrate an alternative embodiment (with like elements being labeled with like reference numerals to those used in connection with the embodiment of Fig. 1) wherein the arms 24 are flipped to the other side of the body 18. The modified arms 24 are designed to permit the tendons (not shown) to pass by them and engage with the cortical bone. The arm-to-body joint is a pin-less design with a track way in the body that secures the arm 24 in place.

25 Figs. 16A and 16B illustrate yet another modified embodiment wherein, once again, like elements are labeled with like reference numerals as those used in connection with the earlier embodiments. In this embodiment, the implant 10 uses the body 18 as a wedge.

Testing has been done by the inventors to verify the functionality of the disclosed invention of Figs. 1-7. As shown in Fig. 17, the inventors found that

pull-out forces for the implant 10 were significantly higher than those of a predicate device, the RCI interference screw available from Smith & Nephew.

In Figs. 18-21 there is shown another implant embodiment 110, wherein like elements are identified with like reference numerals as for the embodiment of Figs. 1-14, preceded by the numeral 1. As shown, the deployment screw 112 protrudes through the compression pads 114 and 116, which are each integrated into the body 118. The deployment screw 112 is threaded at its distal end into the wedge 120. Two pins 122 attach a pair of arms 124 to the body 118, as shown.

As noted above, in this embodiment the compression pads 114, 116 are integrated into the body 118. This feature permits the use of a shorter implant than is the case for the implant of Fig. 1. A track 126 in the wedge 120 attaches to track posts 128 on the arms 124 (Fig. 29), which keep the wedge 120 from rotating during deployment. The compression pads expand as the implant is deployed. In particular, the screw 112 expands the pads 114, 116 outwardly by sliding on a compression taper 72 (Fig. 27), as shown in Figs. 20-23. Moreover, as the deployment screw 112 rotates, the wedge 120 expands the arms 124 as also shown in Figs. 20-23. Once the screw 112 is fully seated, the expanded arms 124 fully engage with adjacent cancellous bone 74, thus locking the anchor in place, as shown in Fig. 24.

The deployment screw 112 (Fig. 26) has a male quad lead section 132 with four separate thread starts, as in the prior disclosed embodiment. This means that for every one rotation of the screw, the linear distance it travels is four times that which a single lead screw would travel. This enables the user to turn the screw fewer times than would be required with a single start thread, approximating the same number of turns that the user would need during the implantation of an interference screw such as the RCI screw available from Smith & Nephew. Oftentimes, during implantation, an interference screw such as the RCI screw requires a notch to be placed at the edge of the femoral tunnel aperture to permit the screw to start engaging the bone. However, the present invention avoids the need for such a step, resulting in an easier

implantation procedure. The invention is easy to deploy as an interference screw, and requires fewer steps. The deployment screw 112 also provides a rigid backbone to support the implant. A reverse threaded hex 75 is preferably provided to drive the screw.

5 The screw head or compression pad deployer 134 deploys the compression pads 114, 116 as the screw 112 advances axially into the implant. Another feature of the screw is the provision of a load transfer disk 136 that transfers some of the axial load from the screw head 134 to body junction to the disk to body junction. This allows for thinner side walls or struts 138 on the
10 body 118 due to the decreased load on the struts, which in turn allows a larger tendon to fit between the deployment screw 112 and the body 118.

As shown in Fig. 25, the compression pads 114, 116 compress the tendons 170 against the femoral tunnel wall to promote tendon-to-bone healing at the aperture of the tunnel. Unlike prior art approaches for more intimate
15 tendon-to-bone contact that only reduce the space between the tendon and the tunnel wall, the present invention actively compresses the tendons against the bone tunnel. The compression pads 114, 116 in this embodiment are integral with the body 118.

The body 118 functions to trap the tendons 170 on either side of the
20 deployment screw 112. The struts 138 are split, as shown at reference numeral 76 (Fig. 28), to allow the integrated compression pads 114, 116 to expand and compress the tendon against the bone tunnel. They also provide structural support for the deployment screw 112, wedge 120, and arms 124 to deploy against.

25 The arms 124 include a few key design features, as particularly shown in Figs. 29 and 30. Fins 146 on the top provide torsional strength for the wedge 120 to arm 124 junction. They also allow easier insertion into the femoral tunnel when inserting into a femoral tunnel that is drilled off-axis from the tibial tunnel. The portion of the arm 24 that engages with the bone has a tapered edge
30 148 which allows for ease of bone displacement during deployment. The support rib 150 along the length of the arm 124 is also tapered for ease of bone

displacement and provides structural support during axial loading. The torsion pins 152 engage with a torsion hole 154 to provide additional torsional strength while inserting into the femoral tunnel.

As in the prior embodiment, the wedge 120 is threaded with a female
5 quad lead thread 156 that matches the complementary threads 132 on the deployment screw 112. The track posts 128 on the arms 124 engage with the wedge track 126 to provide torsional strength through deployment. A tapered nose 158 allows easier off-axis insertion into the femoral tunnel.

Fig. 32 is a table similar to that of Fig. 17, presenting data generated by
10 the inventors which indicates that pull-out forces for the implant 110 were significantly higher than those of a predicate device, the RCI interference screw available from Smith & Nephew.

Still another embodiment of the inventive implant is illustrated in Figs. 33-54, wherein like elements to those of the prior embodiments are identified
15 by like reference numerals, preceded by the numeral 2. This embodiment 210 utilizes the cortical bone for fixation in combination with tendon-to-bone compression. In this version of the invention, the deployment screw 212 is offset to one side of the implant 210, for the purpose of permitting easier passing of tendon through the orifice. This implant deploys in two steps.
20 The deployment screw 212 is rotated clockwise as an arm 78 and wedge 220 slide together across tapered faces 80 (Fig. 46) and 82 (Fig. 48) until they lock together with their respective cortical locks 84, 86. The wedge 220 and the arm 78 lock into place by filling a majority of the cross section of the femoral tunnel. Thus, the implant is free to move in the femoral tunnel, allowing tactile
25 feedback to ensure engagement of a cortical tab 88 with the cortex.

The screw is then rotated so that it is advanced the remainder of the way, and the compression wedge 90 engages with the compression pads, thereby pressing the tendon against the bone tunnel wall. A track 92, 94 in the compression pads 214, 216 and compression wedge 90 prevents the
30 compression wedge from engaging unevenly. A progression of deployment of the implant 210 is illustrated in Figs. 35-42. Figs. 43-50 illustrate various

components of the embodiment. In the undeployed state, the arm is engaged with the wedge with the arm's track posts 228 engaging with a T-bar 96 of the wedge 220. This prevents the arm 78 from moving during insertion. Also, to prevent the wedge 220 from rotating during deployment, the track post 228 is
5 inserted into a torsion slot 100.

Modified cortical fixation implant designs are illustrated in Figs. 51-54. Figs. 51 and 52 illustrate a modified wedge and only one arm which allows engagement with the cortical bone. Figs. 53 and 54 illustrate the same embodiments as in Figs. 51 and 52, wherein the screw is to one side of the
10 implant.

Fig. 55 has been incorporated into this application to illustrate a substantially completed ACL repair procedure. Figs. 8 and 9, as well as Figs. 24 and 25 and Figs. 41 and 42, illustrate the installation of the femoral anchor of the present invention, in various embodiments. However, as one skilled in
15 the art would understand, to complete the repair procedure further steps are necessary. Once the femoral anchor has been deployed and installed, as previously described, the anchored tendons 70 extend proximally from the femoral tunnel through the tibial tunnel and out through tibial aperture 66. To complete the procedure, a tibial anchor 102 is preferably installed, to anchor the
20 tendon bundles in place, as shown in Fig. 55. Once this anchor is in place, the proximal ends of the tendon bundles are trimmed to complete the procedure. This portion of the ACL reconstruction procedure is fully explained in co-pending U.S. Application Serial No. 11/725,981, which has already been fully and expressly incorporated by reference herein. Any suitable tibial anchor 102
25 may be used in conjunction with femoral anchors of the type disclosed in this application, but the tibial anchors shown and described in the '981 patent application are presently preferred.

Accordingly, although exemplary embodiments of the invention has been shown and described, it is to be understood that all the terms used herein are
30 descriptive rather than limiting, and that many changes, modifications, and

substitutions may be made by one having ordinary skill in the art without departing from the spirit and scope of the invention.

CLAIMS:

1. A material fixation system, comprising:
 - an implant comprising a body having a distal end and a proximal end which is placeable in a tunnel disposed in a portion of bone, wherein the tunnel is defined by walls comprised of bone;
 - a first member which is deployable outwardly to engage adjacent bone for anchoring said implant in place in the tunnel;
 - a second member which is deployable outwardly to engage tissue material to be fixed within said tunnel, and to move the tissue material outwardly into contact with the tunnel walls, wherein said second member comprises blunt tissue engaging surfaces which engage the tissue without piercing it; and
 - a third member which is movable generally axially to deploy said first member outwardly.
2. The material fixation system as recited in Claim 1, wherein said first member comprises a surface which is angled relative to a longitudinal axis of said implant body, said angled surface being adapted to anchor the implant by engaging cortical bone.
3. The material fixation system as recited in Claim 1, and further comprising a fourth member for actuating said third member to move in order to deploy said first member.
4. The material fixation system as recited in Claim 3, wherein said fourth member comprises a portion which functions to deploy said second member outwardly.
5. The material fixation system as recited in Claim 1, wherein said first member is disposed on said body.
6. The material fixation system as recited in Claim 5, wherein said first member comprises an arm which is pivotally attached to said body.
7. The material fixation system as recited in Claim 6, wherein said third member comprises a wedge which is movable generally axially to deploy said arm.
8. The material fixation system as recited in Claim 7, wherein said fourth member comprises a deployment screw having a distal end and a proximal end, said deployment screw

being adapted to extend axially through said body, the distal end of said deployment screw having a threaded portion which is engageable with a complementary threaded portion on said wedge, wherein rotation of said deployment screw causes relative movement of said deployment screw and said wedge.

9. The material fixation system as recited in Claim 8, wherein said wedge moves proximally to deploy said arm.

10. The material fixation system as recited in Claim 7, wherein said second member comprises a compression pad.

11. The material fixation system as recited in Claim 10, wherein said fourth member portion comprises a head of said deployment screw, disposed on the proximal end thereof.

12. An implant system for use in making an orthopedic repair of a joint, said implant system comprising:

a first implant adapted for receiving a tissue graft thereon and then being disposed in a first bone tunnel location, wherein ends of the tissue graft extend through a bone tunnel and out of a proximal end of the tunnel, said first implant comprising:

a body portion having a distal end and a proximal end;

a first member disposed on said body portion which is deployable outwardly to engage adjacent bone for anchoring said implant place in the tunnel;

a second member disposed on said body portion which comprises blunt surfaces that are deployable outwardly to engage tissue material to be fixed within said tunnel, and to move the tissue material outwardly into contact with the tunnel walls without piercing the tissue or the tunnel walls;

a third member comprising a wedge which is movable generally axially to deploy said first member outwardly; and

a fourth member for actuating said third member to move in order to deploy said first member; and

a second implant adapted for disposition in a second bone tunnel location, proximal to said first bone tunnel location, said second implant being adapted to secure the ends of the tissue graft which extend from the first implant against adjacent bone.

13. The implant system as recited in Claim 12, wherein said fourth member comprises a portion which functions to deploy said second member outwardly.
14. The implant system as recited in Claim 12, wherein said first member comprises an arm which is pivotally attached to said body.
15. The implant system as recited in Claim 12 or 14, wherein said fourth member comprises a deployment screw having a distal end and a proximal end, said deployment screw being adapted to extend axially through said body, the distal end of said deployment screw having a threaded portion which is engageable with a complementary threaded portion on said wedge, wherein rotation of said deployment screw causes relative movement of said deployment screw and said wedge.
16. The implant system as recited in Claim 15 when appended to claim 14, wherein said wedge moves proximally to deploy said arm.
17. The implant system as recited in Claim 12 or 15, wherein said second member comprises a compression pad.
18. The implant system as recited in Claim 15, wherein said fourth member portion comprises a head of said deployment screw, disposed on the proximal end thereof.
19. A material fixation system substantially as hereinbefore described with reference to any one of the embodiments as that embodiment is shown in the accompanying drawings.
20. An implant system substantially as hereinbefore described with reference to any one of the embodiments as that embodiment is shown in the accompanying drawings.

Dated 7 February 2013
Cayenne Medical, Inc
Patent Attorneys for the Applicant/Nominated Person
SPRUSON & FERGUSON

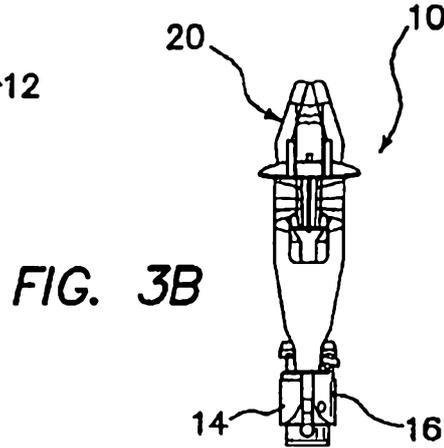
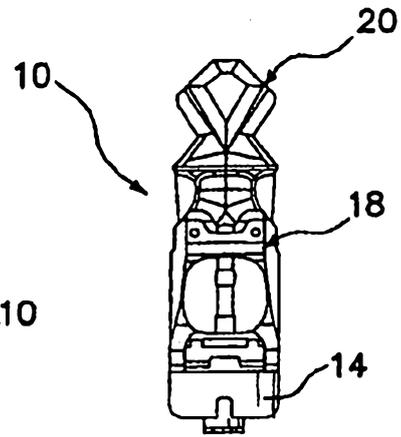
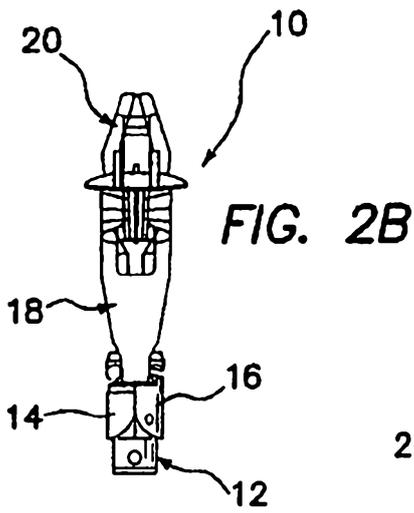
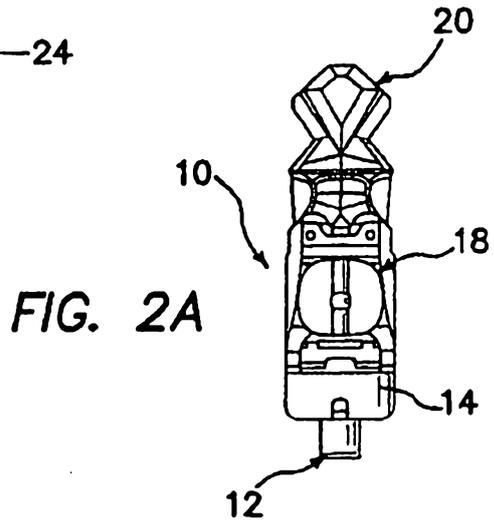
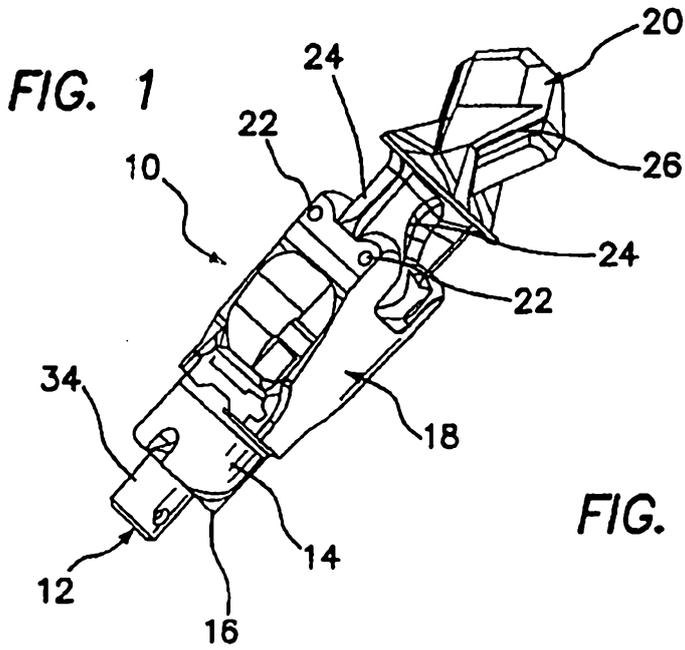
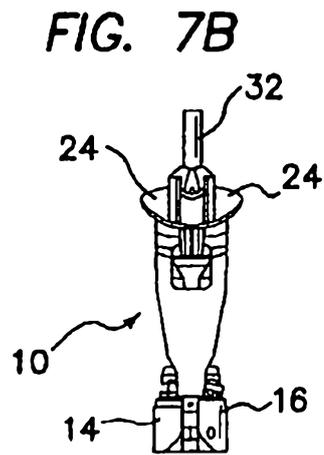
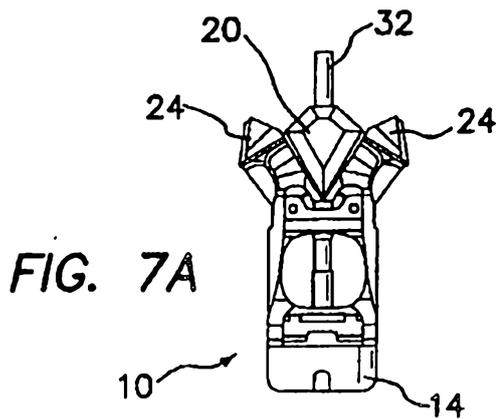
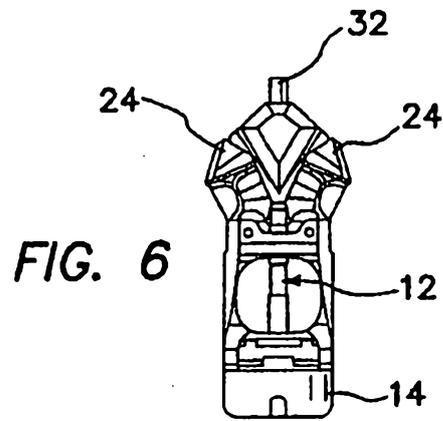
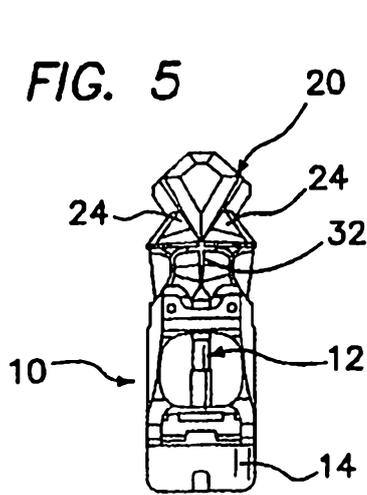
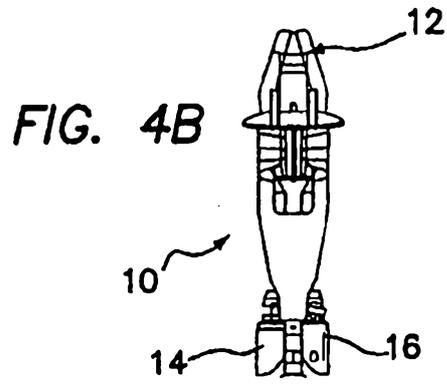
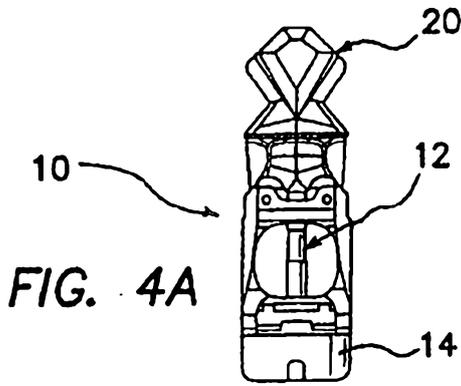


FIG. 3A

FIG. 3B



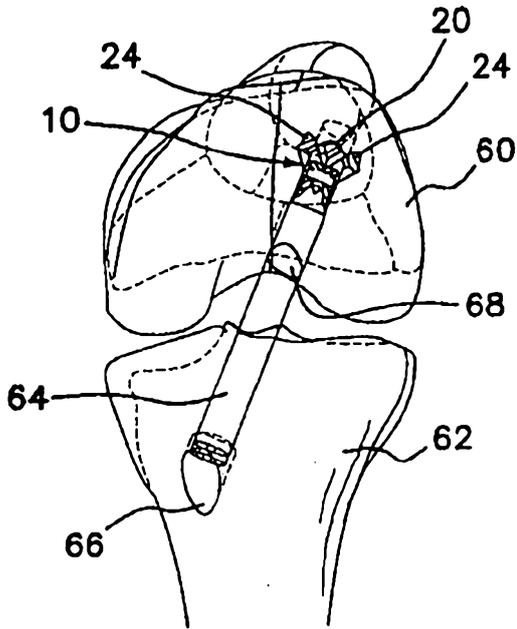


FIG. 8

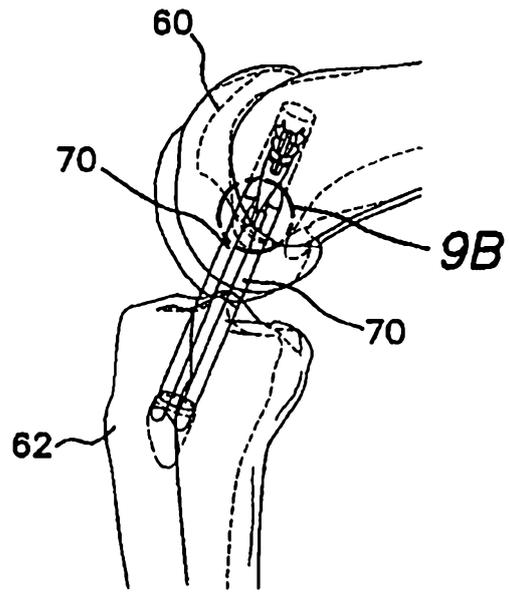


FIG. 9A

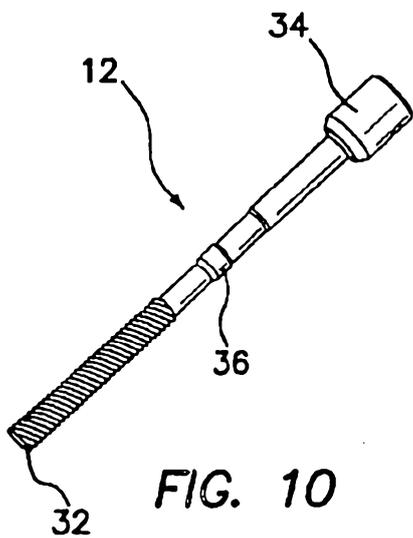


FIG. 10

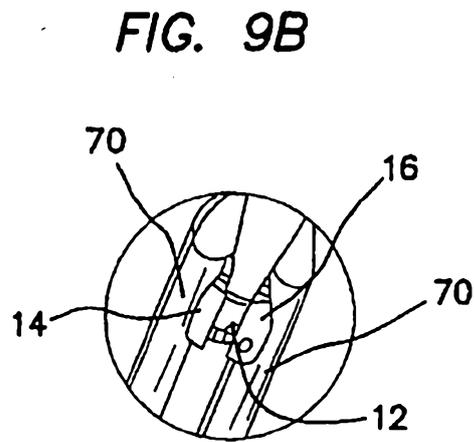


FIG. 9B

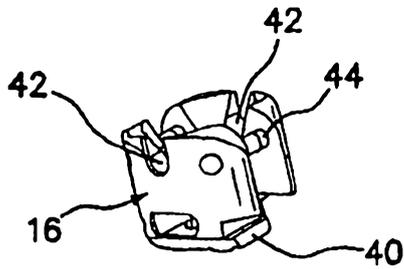


FIG. 11A

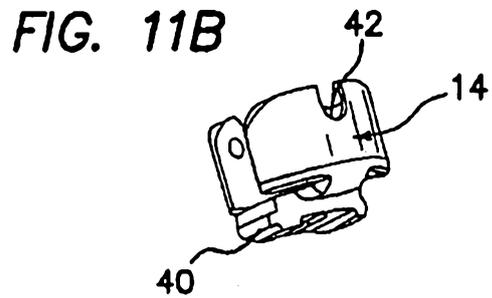


FIG. 11B

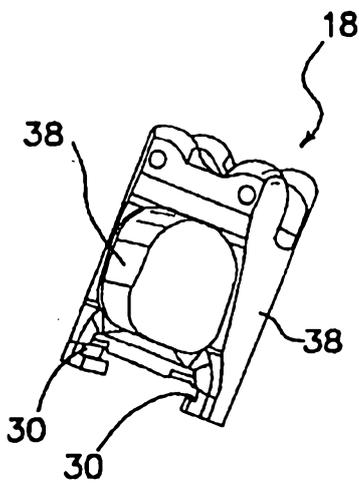


FIG. 12

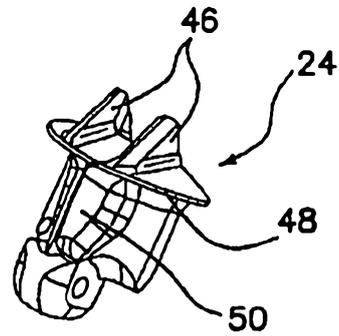


FIG. 13A

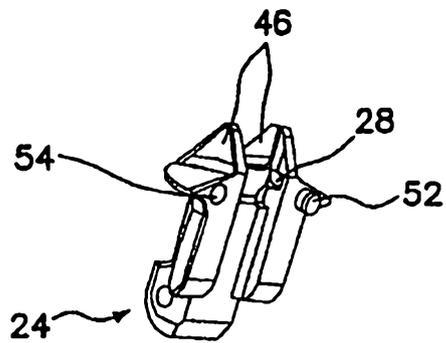


FIG. 13B

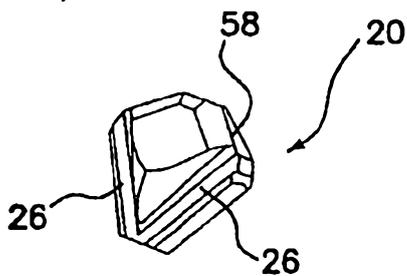


FIG. 14A

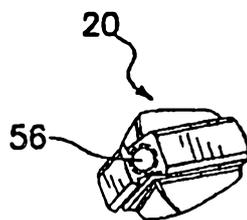


FIG. 14B

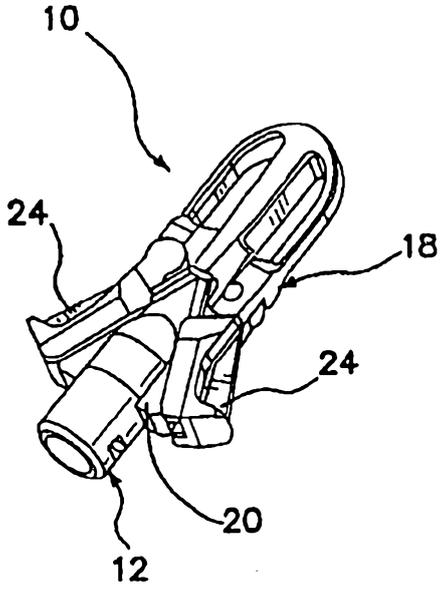


FIG. 15A

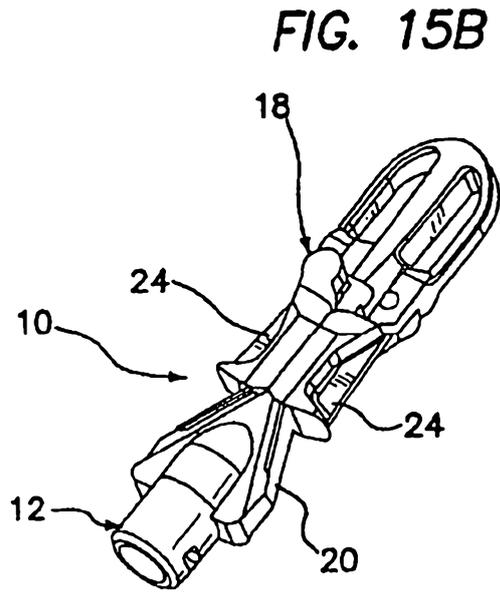


FIG. 15B

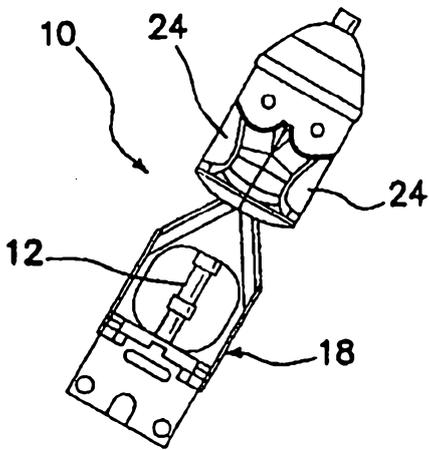


FIG. 16A

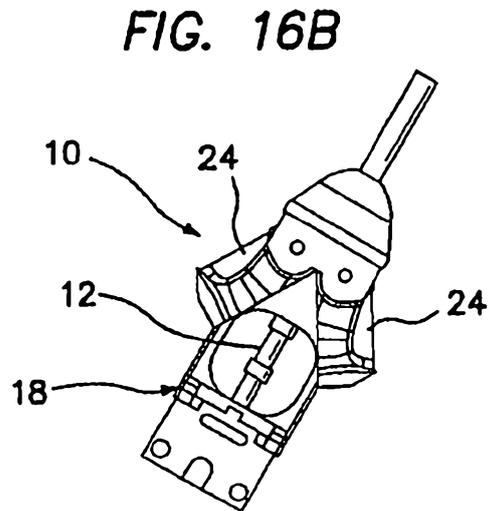


FIG. 16B

		Pull out Forces (N)
Implants	Mean	1253
	Standard Deviation	142.5
	Minimum Value	938.3
	Maximum value	1567.9
		Pull out Forces (N)
RCI Screws	Mean	532.7
	Standard Deviation	349.7
	Minimum Value	135.7
	Maximum value	1230.9

FIG. 17

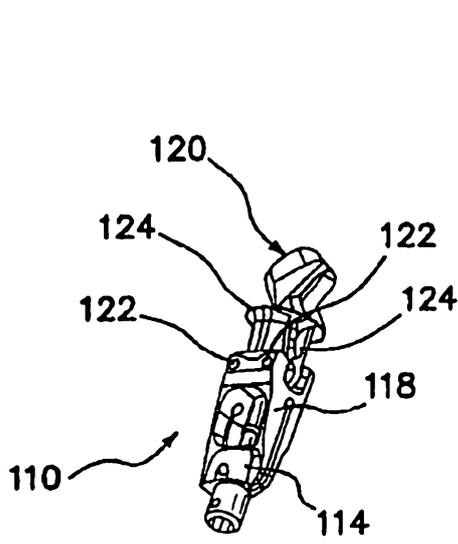


FIG. 18

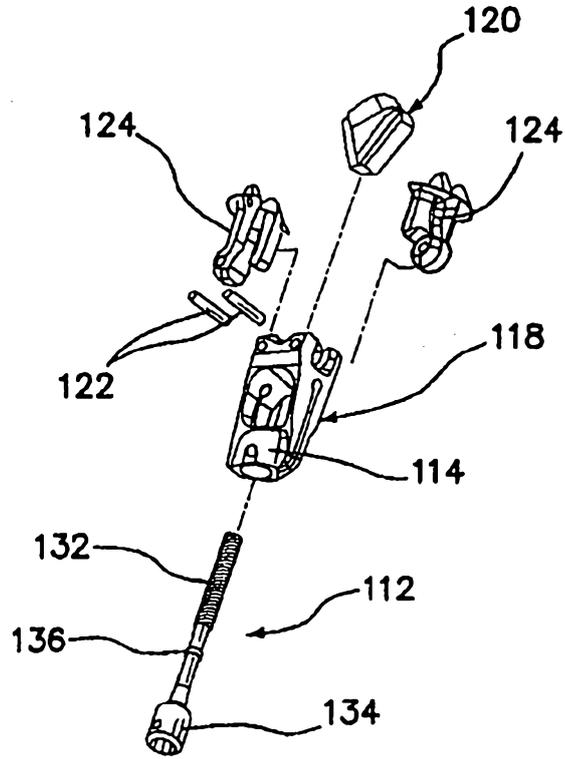


FIG. 19

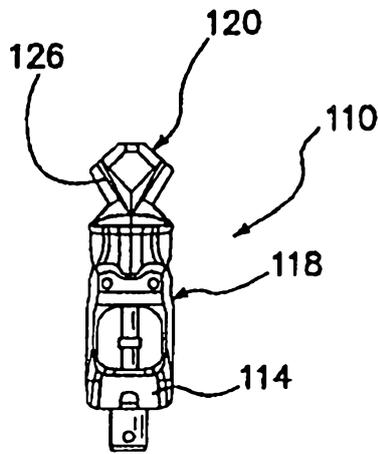


FIG. 20

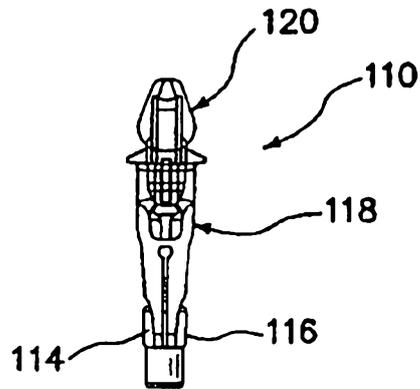


FIG. 21

FIG. 22

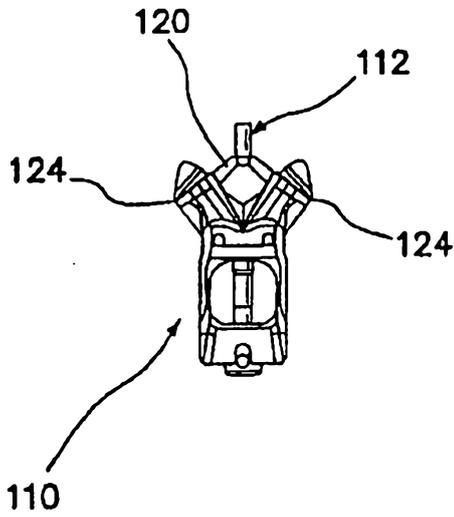


FIG. 23

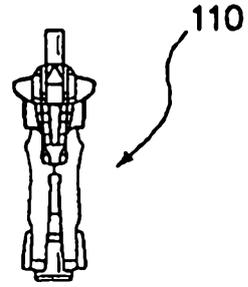
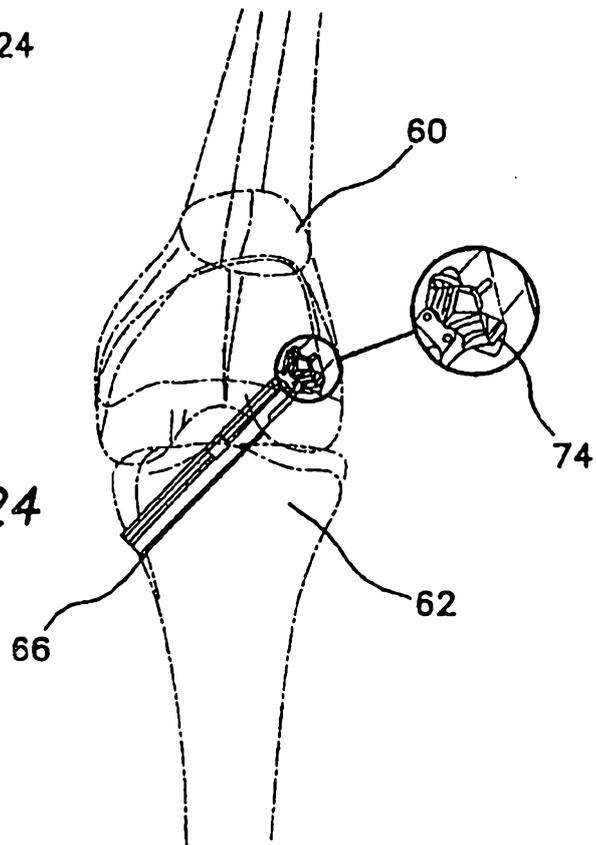


FIG. 24



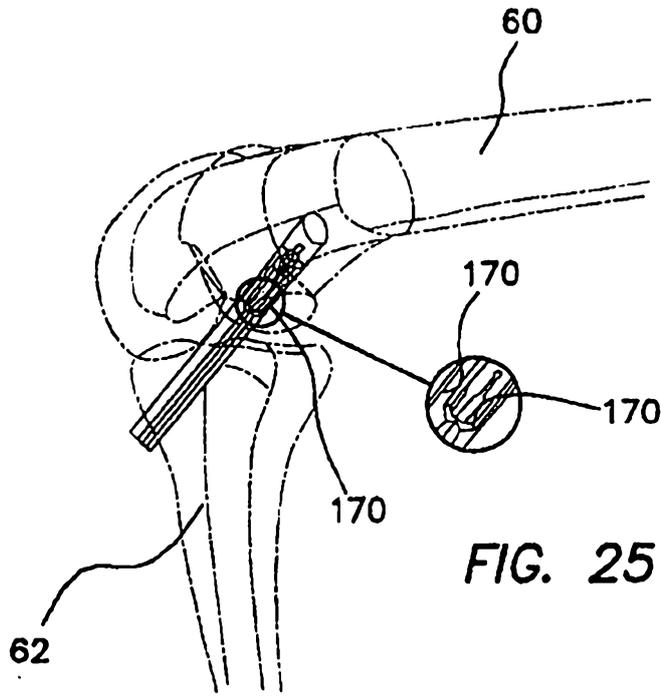


FIG. 25

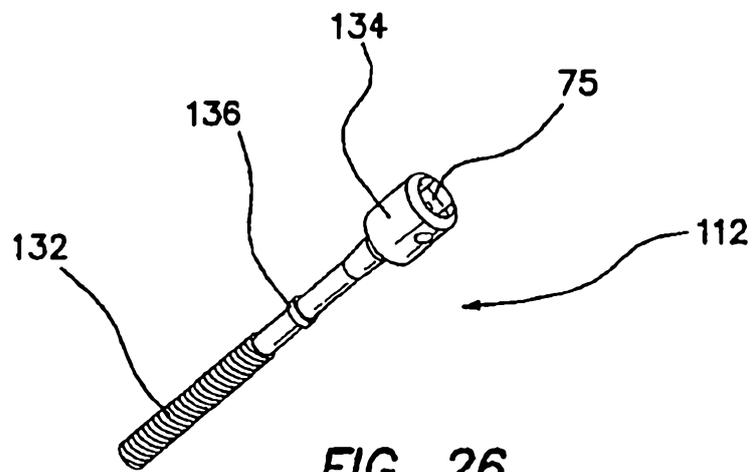


FIG. 26

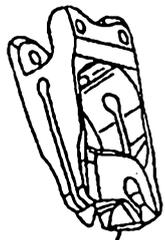


FIG. 27

72



FIG. 28

138

138

76

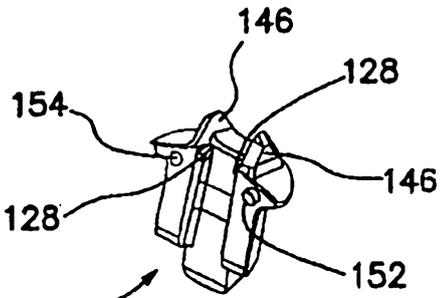


FIG. 29

154

146

128

128

146

152

124

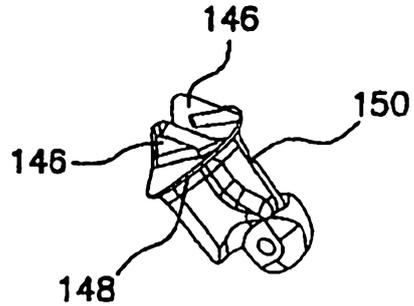


FIG. 30

146

146

150

148

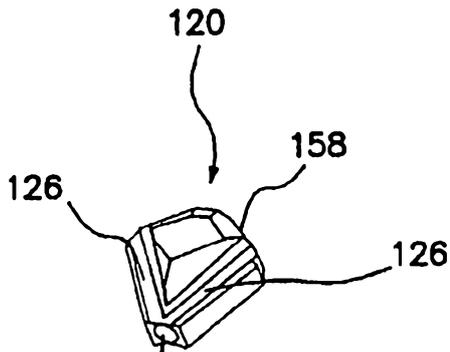


FIG. 31

120

126

158

126

156

		Pull out Forces (N)
Cancellous Implant	Mean	1164.2
	Standard Deviation	215.9
	Minimum Value	728
	Maximum Value	1643
		Pull out Forces (N)
RCI Screws	Mean	532.7
	Standard Deviation	349.7
	Minimum Value	135.7
	Maximum Value	1230.9

FIG. 32

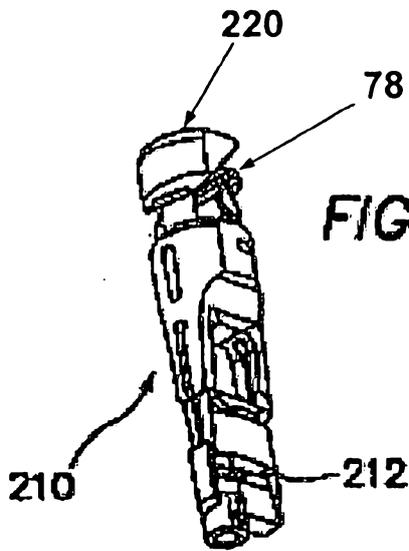


FIG. 33

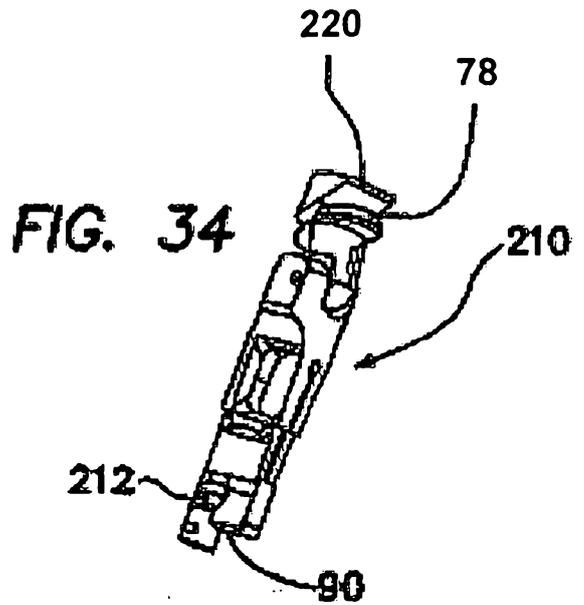


FIG. 34

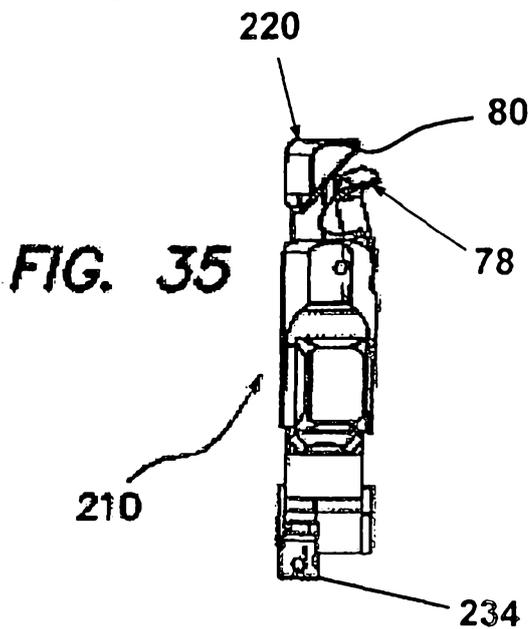


FIG. 35

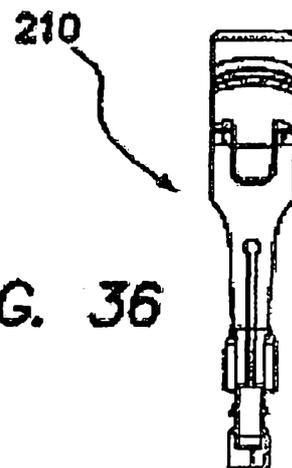


FIG. 36

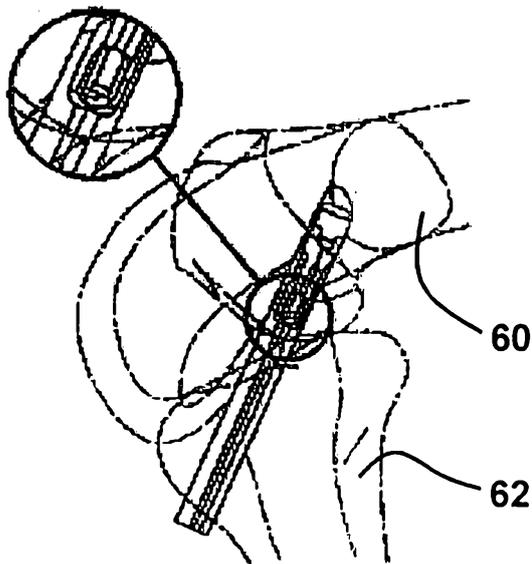
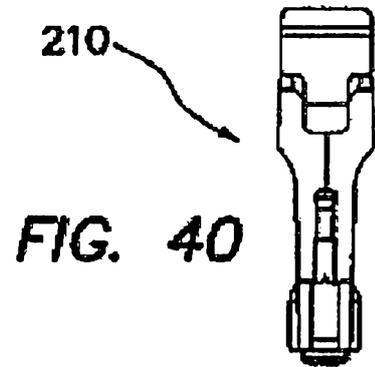
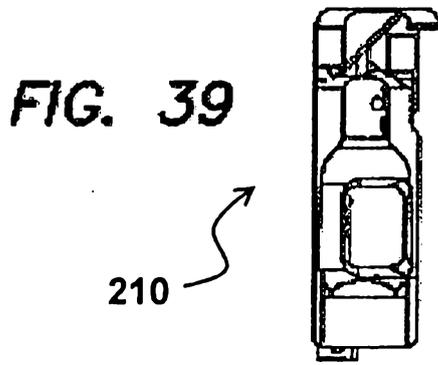
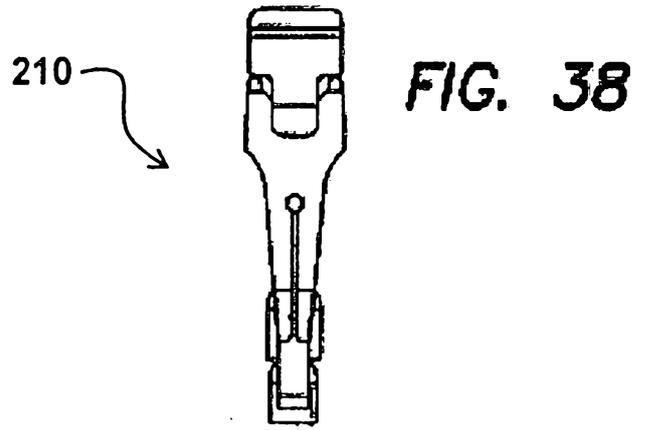
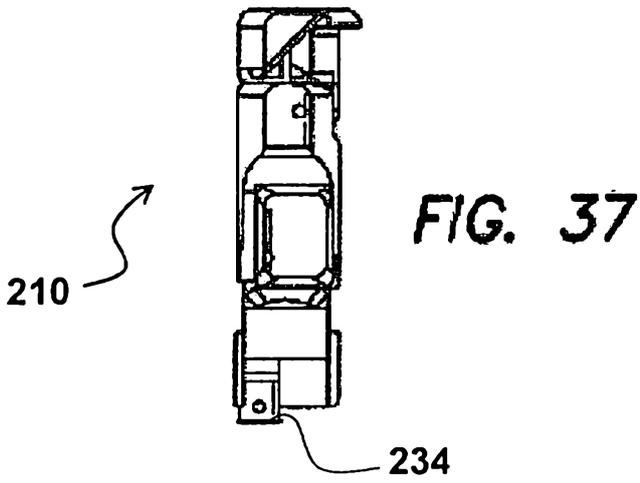


FIG. 41

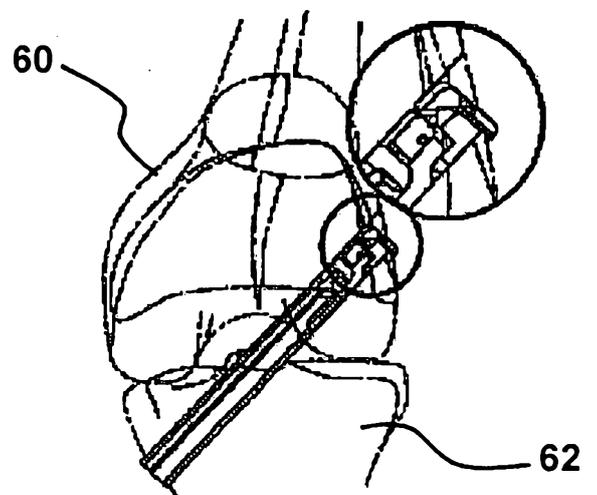


FIG. 42

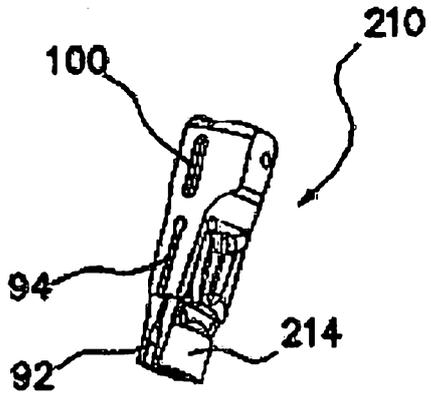


FIG. 43

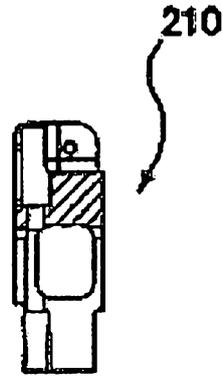


FIG. 44

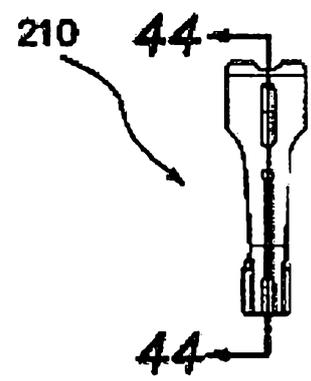


FIG. 45

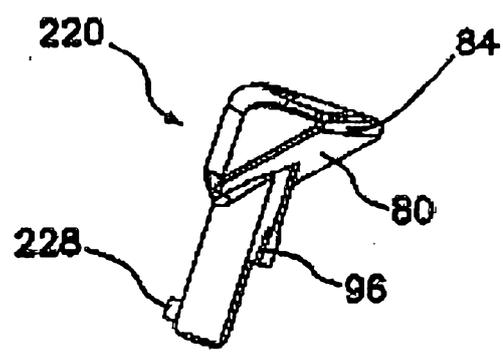


FIG. 46

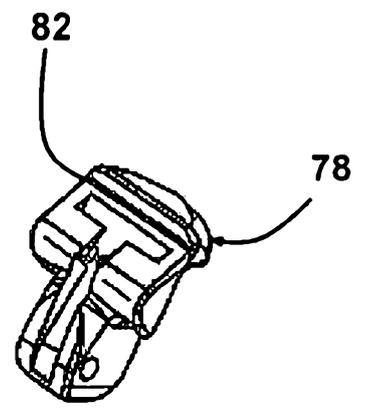


FIG. 47

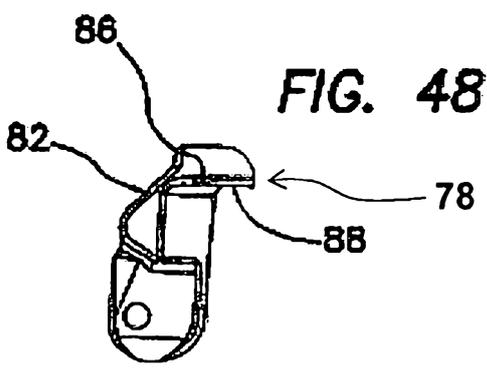


FIG. 48

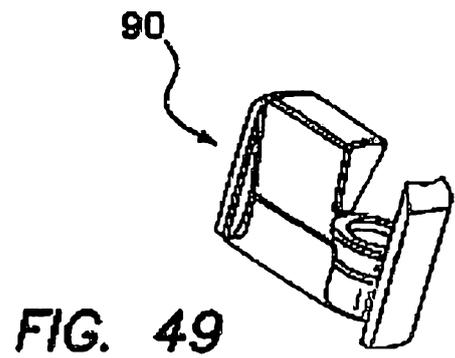
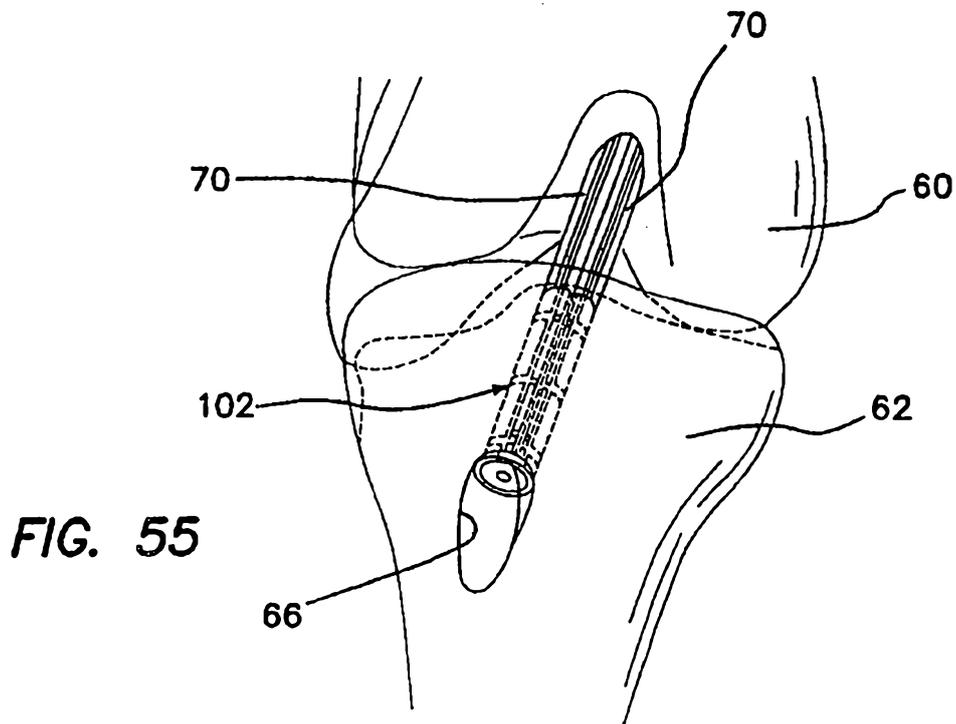
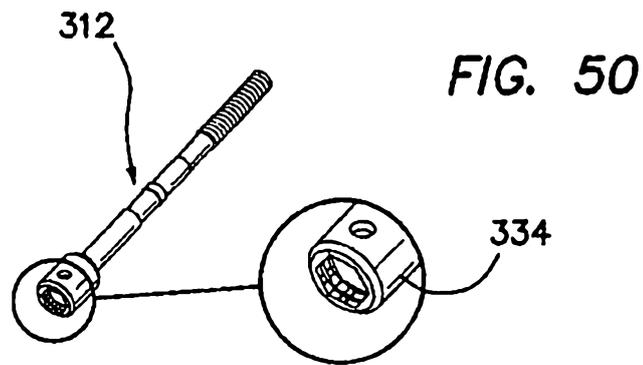


FIG. 49



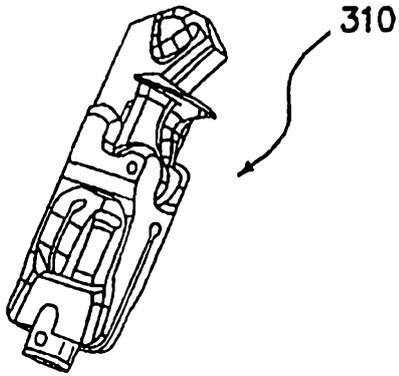


FIG. 51

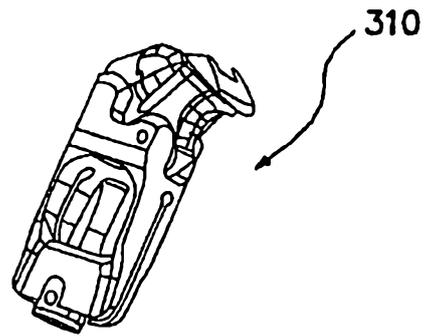


FIG. 52

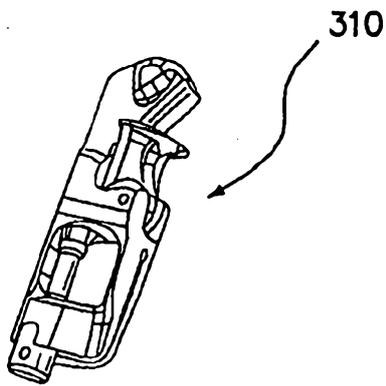


FIG. 53

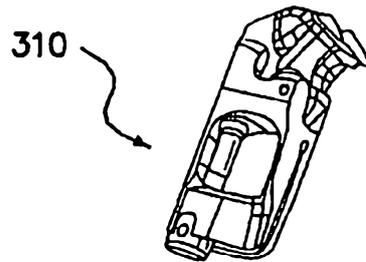


FIG. 54