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(54) Titre : MATERIAUX ET COMPOSITIONS A BASE DE CYCLODEXTRINE, ET UTILISATIONS CORRESPONDANTES
(54) Title: CYCLODEXTRIN-BASED MATERIALS, COMPOSITIONS AND USES RELATED THERETO

(57) **Abrégé/Abstract:**

The application discloses cyclodextrin-modified materials for carrying drugs and other active agents, such as nucleic acids. Compositions are also disclosed of cyclodextrin-modified materials that release such active agents under controlled conditions. The invention also discloses compositions of cyclodextrin-modified polymer carriers that are coupled to biorecognition molecules for assisting the delivery of drugs to their site of action.



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(54) Title: CYCLODEXTRIN-BASED MATERIALS, COMPOSITIONS AND USES RELATED THERETO

(57) Abstract: The application discloses cyclodextrin-modified materials for carrying drugs and other active agents, such as nucleic acids. Compositions are also disclosed of cyclodextrin-modified materials that release such active agents under controlled conditions. The invention also discloses compositions of cyclodextrin-modified polymer carriers that are coupled to biorecognition molecules for assisting the delivery of drugs to their site of action.



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CYCLODEXTRIN-BASED MATERIALS, COMPOSITIONS AND USES RELATED THERETO

Background of the Invention

5 Polymers having pendant sugar moieties known as "glycopolymers"
(Bioconj. Chem., 3:256 (1992)) have attracted much interest in recent years, largely
as scaffolds for the multivalent display of biologically important carbohydrate
molecules. These glycopolymers have been used as potent inhibitors of viral-host
cell attachment and leukocyte-endothelial cell adhesion (FEBS, 272:209 (1990);
10 Can. J. Microbiol., 37:233 (1991); J. Am. Chem. Soc., 119:3161 (1997)).
Glycopolymers have also been explored as vehicles for targeted drug and gene
delivery (J. Hepatology, 21:806 (1994)), and as artificial substrates for cell adhesion
(J. Cell Biol., 115:485 (1991)). The suitability of glycopolymers as biocompatible
implant materials has been relatively unexplored and is limited to a few examples
15 described, for example, in Microbiol. Chem. Phys., 195:3597 (1994).

For polymers used as biocompatible implant materials, their properties,
particularly the surface composition, are of great importance. Efforts include
introducing biocompatible components into the bulk system and on their surface.
Studies described, for example, in J. Colloid Interface Sci., 149:84 (1992) have
20 shown that copolymers with a pendant glucose unit in the bulk or surfaces with
covalently bound neutral polysaccharides demonstrate the reduction of platelet
adhesion and protein adsorption.

Accordingly, biocompatible polymeric materials that are easily prepared
would be useful for drug delivery and other biomedical uses.

25 Summary of the Invention

This invention provides a material formed by crosslinking a polymer bearing
inclusion hosts (such as cyclodextrin) with a linking molecule bearing at least two
functional groups that, as inclusion guests, form inclusion complexes with the
inclusion host. For polymers in which cyclodextrin is the inclusion host, exemplary

inclusion guests include naphthol, adamantane, cholesterol, and derivatives thereof. In certain embodiments, the polymer bears inclusion guests, and linking molecules bearing inclusion hosts such as cyclodextrin are used to crosslink the polymer. Materials according to the above description can be used to deliver therapeutic
5 agents, such as proteins, nucleic acids, and pharmaceuticals.

Brief Description of the Drawings

Figure 1 schematically depicts a crosslinked polymer matrix of the present invention.

Figure 2 illustrates a matrix of the invention including therapeutic moieties.

10 Figure 3 depicts molecular weights of CD-PEG₃₄₀₀ as a function of polymerization times.

Figure 4 presents results of transfection experiments.

Figure 5 shows cell migration through a matrix as described herein.

15 Figure 6 shows a dynamic frequency sweep of CD-PEG₃₄₀₀ polymer without cross-linking. Concentration was 100 mg/ml in PBS, temperature was 37 °C and strain was 0.5%.

Figure 7 presents a dynamic frequency sweep of CD-PEG₃₄₀₀ polymer without cross linker. Concentration was 100 mg/ml in PBS, temperature was 20 °C and strain was 0.5%.

20 Figure 8 provides a dynamic frequency sweep of CD-PEG₃₄₀₀ polymer (100 mg/ml) with 36.5 mg/ml of di-Adamantane-PEG cross linker. Temperature was 37 °C and strain was 0.5%.

Figure 9 is a dynamic frequency sweep of CD-PEG₃₄₀₀ polymer (100 mg/ml) with 36.5 mg/ml of di-Adamantane-PEG cross linker. Temperature was 20 °C and
25 strain was 0.5%.

Figure 10 shows a dynamic frequency sweep of bovine collagen matrix at 2.4 mg/ml. Temperature was 37 °C and strain was 0.5%.

Figure 11 illustrates results of in vitro assays using a matrix as described herein.

5 Figure 12 portrays results of treating wounds with subject compositions.

(12A): ICR mouse treated with Matrix A (Left Wound) and Matrix B (Right Wound). Animal shown at sacrifice 4 days post surgery. The purple ink is markings from a surgical pen and not the dye (dark blue/black in color) used in the matrices. Little dye remains on the actual wound site; however, the remaining dye comes from
10 oozing and spreading of the matrices to the surrounding unwounded tissues that occurred after applying the wound dressing. (12B): ICR mouse treated with Matrix A (Left Wound) and Matrix B (Right Wound). Animal shown at sacrifice 4 days post surgery. The left and right wounds show that Matrix A and Matrix B respectively, did not spread to surrounding tissues after injection.

15 Figure 13 shows results of treating wounds with subject compositions.

(13A): ICR mouse treated with Matrix A (Left Wound) and Matrix B (Right Wound). Animal shown at sacrifice 4 days post surgery. Natural wound contraction can be seen in both left and right wounds. A small amount of dye remaining from the original injections can be seen; however, there is no dye present in the
20 surrounding unwounded tissues. (13B): ICR mouse treated with Matrix A (Left Wound) and Matrix B (Right Wound). Animal shown at sacrifice 4 days post surgery. The left and right wounds show that Matrix A and Matrix B, respectively, did not spread to surrounding tissues after injection.

Figure 14 depicts PDGF-B expression levels within treated sponges. QRT-
25 PCR was performed on individual sponge samples from each treatment group. The data is expressed as the average of 6 sponges assayed \pm standard deviation.

Figure 15 illustrates GAPDH RNA levels within treatment groups.

Figure 16 shows viral PDGF-B DNA within treated sponges. QPCR assays were performed on sponge samples from each treatment group. PCR primers targeted specific expression of human PDGF-B sequence and do not cross react with rat PDGF-B DNA.

5 Figure 17 portrays GAPDH DNA content within sponges.

Figure 18 depicts viral hexon DNA within sponge treatment groups.

Figure 19 provides morphological analysis of PVA sponges.

Detailed Description of the Invention

I. Overview

10 Cyclodextrins have a ring structure which has a basket-like shape. This shape allows cyclodextrins to include many kinds of molecules into their internal cavity. See, for example, Szejtli, *Cyclodextrins and Their Inclusion Complexes*; Akademiai Klado, Budapest, 1982; and Bender et al., *Cyclodextrin Chemistry*, Springer-Verlag, Berlin, 1978. Cyclodextrins are able to form inclusion complexes with an array of
15 organic molecules including, for example, drugs, pesticides, herbicides, and agents of war. See, Tenjarla et al., *J. Pharm. Sci.*, 87: 425-429 (1998); Zughul et al., *Pharm. Dev. Technol.*, 3: 43-53 (1998); and Albers et al., *Crit. Rev. Ther. Drug Carrier Syst.*, 12: 311-337 (1995).

Linear cyclodextrin-based polymers (CDPs) have previously been shown to
20 have low toxicity both in vitro (in many different cell lines) and in vivo (Gonzalez et al. 1999 Bioconjugate Chem 10:1068-1074; and Hwang et al. 2001 Bioconjugate Chem 12(2):280-290). The present invention relates, at least in part, to biocompatible materials based on polymers that bear or include cyclodextrin moieties, by crosslinking the linear strands with linking molecules bearing two or
25 more moieties that form inclusion complexes with cyclodextrin, as shown in Figure 1. Additionally, those of skill in the art will recognize that this concept can naturally be extended to polymers bearing or including inclusion hosts other than cyclodextrin, in conjunction with linking molecules that bear inclusion guests that

form inclusion complexes with those inclusion hosts, or, alternatively, polymers that bear inclusion guests in conjunction with linking molecules that bear or include inclusion hosts that form inclusion complexes with those inclusion guests. Examples of inclusion hosts other than cyclodextrins and related cycloamyloses include
5 perhydrotriphenylene (which forms inclusion complexes with polyethylene), urea/thiourea (which form inclusion complexes with fatty acids and related molecules as described in U.S. Patent Nos. 4,776,984, 5,106,542, and 4,170,601), cyclophanes (such as those described in U.S. Patent No. 4,116,955), and those described in U.S. Patent Nos. 4,841,081, 4,367,072, and 4,898,654, all of which are
10 hereby incorporated by reference in their entireties.

In certain embodiments of the present invention, such as is described below in Example 19, a polymer bears both inclusion hosts and inclusion guests, and thus crosslinks with itself by forming inclusion complexes between hosts and guests on the same polymer chain and/or between hosts and guests on adjacent polymer chains.
15 Conditions under which the crosslinking is performed will influence the balance between these two types of inclusion complexes. For example, performing the complexation at high dilution will favor the formation of intramolecular complexes, while performing the complexation at high concentrations will favor the formation of intermolecular complexes, including, in some cases, catenane- and rotaxane-type
20 structures. In certain such embodiments, a high degree of intermolecular interaction increases the rigidity, melting point, and strength of the material.

For purposes of the present application, polymers 'incorporate' inclusion hosts, such as cyclodextrin moieties, by having inclusion hosts within the polymer chain, e.g., removing inclusion hosts from the polymer would require severing the
25 polymer chain. Examples of such polymers are the linear cyclodextrin-based polymers referred to above. Polymers that 'bear' cyclodextrin moieties have a polymer chain to which inclusion hosts are attached, e.g., inclusion hosts are appended to a distinct polymer chain. Polyethylenimine-CD polymers as described herein are examples of this type of polymer. Polymers that 'include' inclusion hosts
30 are those polymers that 'bear' or 'incorporate', or both bear and incorporate, inclusion hosts, or otherwise have covalently bound inclusion hosts as part of the

polymer chain. Any polymer that includes inclusion hosts can be employed in the present application. In certain embodiments, a polymer that incorporates inclusion hosts is a linear (i.e., non-branched) polymer. In certain embodiments, inclusion hosts, e.g., incorporated into or borne on the polymer, are regularly spaced
5 throughout or along the polymer.

The physical properties of the resultant material can be varied by selecting moieties that form inclusion complexes of varying strength; the stronger the complex, the more durable and rigid the resulting material. Similarly, using linking molecules bearing more than two such moieties may increase the strength and
10 rigidity of the material by increasing the degree of crosslinking, as will increasing the proportion of linking molecules to polymer mass. Physical properties of the material can also be varied by altering the flexibility of the linking molecules themselves, or by altering the flexibility of linkers within the cyclodextrin polymer itself.

Furthermore, the in vivo properties of the matrix may be varied by using bonds in the matrix that are labile under physiological conditions. For example, the polymer strands, the crosslinking molecules, or both, may comprise bonds that are labile under physiological conditions, such as ester and peptide bonds. After
15 placement in a physiological environment, these bonds will gradually begin to cleave, resulting in a gradual degradation and loss of structural integrity. A wide spectrum of properties can be achieved by varying the frequency of such bonds in a polymer strand, by combining labile and resistant crosslinking molecules in varying proportions, or by selecting different labile bonds with differing strengths. For
20 example a peptide bond is generally more resistant to cleavage than an ester bond, which is in turn less labile than a thioester bond.
25

Compounds and materials such as therapeutic agents, viruses, adjuvants, and the like, can be formulated with the polymer by forming inclusion complexes, or by simple admixture or encapsulation, without forming inclusion complexes, as is well known in the art for ordinary biocompatible polymers.

30 Compounds increasing the therapeutic utility of the material, such as signaling peptides, other moieties facilitating cell migration, or adjuvants, may be

incorporated into the crosslinked material by conjugating an inclusion complex guest to the entity of interest and including the conjugate in the material as depicted in Figure 2. The conjugate may be included before, during or after the crosslinking process. Therapeutic compounds may also be included in this fashion, preferably
5 where the attachment between the drug and the inclusion guest/host is labile under physiological conditions, such as an ester bond. See U.S. Patent Application Publication Nos. 20030008818 and 20030017972.

II. Definitions

For convenience, certain terms employed in the specification, examples, and
10 appended claims are collected here.

An 'adjuvant', as the term is used herein, is a compound that has little or no therapeutic value on its own, but increases the effectiveness of a therapeutic agent. Exemplary adjuvants include radiosensitizers, transfection-enhancing agents (such as chloroquine and analogs thereof), chemotactic agents and chemoattractants, peptides
15 that modulate cell adhesion and/or cell mobility, cell permeabilizing agents, inhibitors of multidrug resistance and/or efflux pumps, etc.

The terms "biocompatible polymer" and "biocompatibility" when used in relation to polymers are art-recognized. For example, biocompatible polymers include polymers that are neither themselves toxic to the host (e.g., an animal or
20 human), nor degrade (if the polymer degrades) at a rate that produces monomeric or oligomeric subunits or other byproducts at toxic concentrations in the host. In certain embodiments of the present invention, biodegradation generally involves degradation of the polymer in an organism, e.g., into its monomeric subunits, which may be known to be effectively non-toxic. Intermediate oligomeric products
25 resulting from such degradation may have different toxicological properties, however, or biodegradation may involve oxidation or other biochemical reactions that generate molecules other than monomeric subunits of the polymer. Consequently, in certain embodiments, toxicology of a biodegradable polymer intended for in vivo use, such as implantation or injection into a patient, may be

determined after one or more toxicity analyses. It is not necessary that any subject composition have a purity of 100% to be deemed biocompatible. Hence, a subject composition may comprise 99%, 98%, 97%, 96%, 95%, 90% 85%, 80%, 75% or even less of biocompatible polymers, e.g., including polymers and other materials
5 and excipients described herein, and still be biocompatible.

To determine whether a polymer or other material is biocompatible, it may be necessary to conduct a toxicity analysis. Such assays are well known in the art. One example of such an assay may be performed with live carcinoma cells, such as GT3TKB tumor cells, in the following manner: the sample is degraded in 1 M
10 NaOH at 37 °C until complete degradation is observed. The solution is then neutralized with 1 M HCl. About 200 µL of various concentrations of the degraded sample products are placed in 96-well tissue culture plates and seeded with human gastric carcinoma cells (GT3TKB) at 104/well density. The degraded sample products are incubated with the GT3TKB cells for 48 hours. The results of the assay
15 may be plotted as % relative growth vs. concentration of degraded sample in the tissue-culture well. In addition, polymers and formulations of the present invention may also be evaluated by well-known in vivo tests, such as subcutaneous implantations in rats to confirm that they do not cause significant levels of irritation or inflammation at the subcutaneous implantation sites.

20 The term "biodegradable" is art-recognized, and includes polymers, compositions and formulations, such as those described herein, that are intended to degrade during use. Biodegradable polymers typically differ from non-biodegradable polymers in that the former may be degraded during use. In certain embodiments, such use involves in vivo use, such as in vivo therapy, and in other certain
25 embodiments, such use involves in vitro use. In general, degradation attributable to biodegradability involves the degradation of a biodegradable polymer into its component subunits, or digestion, e.g., by a biochemical process, of the polymer into smaller, non-polymeric subunits. In certain embodiments, two different types of biodegradation may generally be identified. For example, one type of biodegradation
30 may involve cleavage of bonds (whether covalent or otherwise) in the polymer

backbone. In such biodegradation, monomers and oligomers typically result, and even more typically, such biodegradation occurs by cleavage of a bond connecting one or more of subunits of a polymer. In contrast, another type of biodegradation may involve cleavage of a bond (whether covalent or otherwise) internal to sidechain
5 or that connects a side chain to the polymer backbone. For example, a therapeutic agent or other chemical moiety attached as a side chain to the polymer backbone may be released by biodegradation. In certain embodiments, one or the other or both general types of biodegradation may occur during use of a polymer.

As used herein, the term "biodegradation" encompasses both general types of
10 biodegradation. The degradation rate of a biodegradable polymer often depends in part on a variety of factors, including the chemical identity of the linkage responsible for any degradation, the molecular weight, crystallinity, biostability, and degree of cross-linking of such polymer, the physical characteristics (e.g., shape and size) of an implant, and the mode and location of administration. For example, the greater the
15 molecular weight, the higher the degree of crystallinity, and/or the greater the biostability, the biodegradation of any biodegradable polymer is usually slower. The term "biodegradable" is intended to cover materials and processes also termed "bioerodible".

In certain embodiments wherein the biodegradable polymer also has a
20 therapeutic agent or other material associated with it, the biodegradation rate of such polymer may be characterized by a release rate of such materials. In such circumstances, the biodegradation rate may depend on not only the chemical identity and physical characteristics of the polymer, but also on the identity of material(s) incorporated therein. Degradation of the subject compositions includes not only the
25 cleavage of intramolecular bonds, e.g., by oxidation and/or hydrolysis, but also the disruption of intermolecular bonds, such as dissociation of host/guest complexes by competitive complex formation with foreign inclusion hosts.

In certain embodiments, polymeric formulations of the present invention biodegrade within a period that is acceptable in the desired application. In certain
30 embodiments, such as in vivo therapy, such degradation occurs in a period usually

less than about five years, one year, six months, three months, one month, fifteen days, five days, three days, or even one day on exposure to a physiological solution with a pH between 6 and 8 having a temperature of between 25 and 37 °C. In other embodiments, the polymer degrades in a period of between about one hour and
5 several weeks, depending on the desired application.

A biohydrolyzable bond (e.g., ester, amide, carbonate, carbamates, or imide) refers to a bond that is cleaved (e.g., an ester is cleaved to form a hydroxyl and a carboxylic acid) under physiological conditions. Physiological conditions include the acidic and basic environments of the digestive tract (e.g., stomach, intestines,
10 etc.), acidic environment of a tumor, enzymatic cleavage, metabolism, and other biological processes, and preferably refer to physiological conditions in a vertebrate, such as a mammal.

The term "healthcare providers" refers to individuals or organizations that provide healthcare services to a person, community, etc. Examples of "healthcare
15 providers" include doctors, hospitals, continuing care retirement communities, skilled nursing facilities, subacute care facilities, clinics, multispecialty clinics, freestanding ambulatory centers, home health agencies, and HMO's.

"Instruction(s)" as used herein means documents describing relevant materials or methodologies pertaining to a kit. These materials may include any
20 combination of the following: background information, list of components and their availability information (purchase information, etc.), brief or detailed protocols for using the kit, trouble-shooting, references, technical support, and any other related documents. Instructions can be supplied with the kit or as a separate member component, either as a paper form or an electronic form which may be supplied on
25 computer readable memory device or downloaded from an internet website, or as recorded presentation. Instructions can comprise one or multiple documents, and are meant to include future updates.

"Kit" as used herein means a collection of at least two components constituting the kit. Together, the components constitute a functional unit for a

given purpose. Individual member components may be physically packaged together or separately. For example, a kit comprising an instruction for using the kit may or may not physically include the instruction with other individual member components. Instead, the instruction can be supplied as a separate member
5 component, either in a paper form or an electronic form which may be supplied on computer readable memory device or downloaded from an internet website, or as recorded presentation.

As used herein, the term 'RNAi construct' is a generic term including small interfering RNAs (siRNAs), hairpin RNAs, and other RNA species which can be
10 cleaved *in vivo* to form siRNAs. RNAi constructs herein also include expression vectors (also referred to as RNAi expression vectors) capable of giving rise to transcripts which form dsRNAs or hairpin RNAs in cells, and/or transcripts which can produce siRNAs *in vivo*.

An 'effective amount' of a subject compound, with respect to the subject
15 method of treatment, refers to an amount of the therapeutic in a preparation which, when applied as part of a desired dosage regimen provides a benefit according to clinically acceptable standards for the treatment or prophylaxis of a particular disorder.

'Patients' or 'subjects' to be treated by the subject method are animals,
20 preferably mammals, including humans.

The term "prophylactic or therapeutic" treatment is art-recognized and includes administration to the host of one or more of the subject compositions. If it is administered prior to clinical manifestation of the unwanted condition (e.g., disease or other unwanted state of the host animal) then the treatment is
25 prophylactic, i.e., it protects the host against developing the unwanted condition, whereas if it is administered after manifestation of the unwanted condition, the treatment is therapeutic, (i.e., it is intended to diminish, ameliorate, or stabilize the existing unwanted condition or side effects thereof).

The term "preventing" is art-recognized, and when used in relation to a condition, such as a local recurrence (e.g., pain), a disease such as cancer, a syndrome complex such as heart failure or any other medical condition, is well understood in the art, and includes administration of a composition which reduces the frequency of, or delays the onset of, symptoms of a medical condition in a subject relative to a subject which does not receive the composition. Thus, prevention of cancer includes, for example, reducing the number of detectable cancerous growths in a population of patients receiving a prophylactic treatment relative to an untreated control population, and/or delaying the appearance of detectable cancerous growths in a treated population versus an untreated control population, e.g., by a statistically and/or clinically significant amount. Prevention of an infection includes, for example, reducing the number of diagnoses of the infection in a treated population versus an untreated control population, and/or delaying the onset of symptoms of the infection in a treated population versus an untreated control population. Prevention of pain includes, for example, reducing the frequency of, or alternatively delaying, pain sensations experienced by subjects in a treated population versus an untreated control population.

As used herein, the terms "therapeutic agent" include any synthetic or naturally occurring biologically active compound or composition of matter which, when administered to an organism (human or nonhuman animal), induces a desired pharmacologic, immunogenic, and/or physiologic effect by local and/or systemic action. The term therefore encompasses those compounds or chemicals traditionally regarded as drugs, vaccines, and biopharmaceuticals including molecules such as proteins, peptides, hormones, nucleic acids, gene constructs and the like. More particularly, the term "therapeutic agent" includes compounds or compositions for use in all of the major therapeutic areas including, but not limited to, adjuvants; anti-infectives such as antibiotics and antiviral agents; analgesics and analgesic combinations, anorexics, anti-inflammatory agents, anti-epileptics, local and general anesthetics, hypnotics, sedatives, antipsychotic agents, neuroleptic agents, antidepressants, anxiolytics, antagonists, neuron blocking agents, anticholinergic and cholinomimetic agents, antimuscarinic and muscarinic agents, antiadrenergics,

antiarrhythmics, antihypertensive agents, hormones, and nutrients, antiarthritics, antiasthmatic agents, anticonvulsants, antihistamines, antinauseants, antineoplastics, antipruritics, antipyretics; antispasmodics, cardiovascular preparations (including calcium channel blockers, beta-blockers, beta-agonists and antiarrhythmics),

5 antihypertensives, diuretics, vasodilators; central nervous system stimulants; cough and cold preparations; decongestants; diagnostics; hormones; bone growth stimulants and bone resorption inhibitors; immunosuppressives; muscle relaxants; psychostimulants; sedatives; tranquilizers; proteins, peptides, and fragments thereof (whether naturally occurring, chemically synthesized or recombinantly produced);

10 and nucleic acid molecules (polymeric forms of two or more nucleotides, either ribonucleotides (RNA) or deoxyribonucleotides (DNA) including both double- and single-stranded molecules, gene constructs, expression vectors, antisense molecules and the like), small molecules (e.g., doxorubicin) and other biologically active macromolecules such as, for example, proteins and enzymes. The agent may be a

15 biologically active agent used in medical, including veterinary, applications and in agriculture, such as with plants, as well as other areas. The term therapeutic agent also includes without limitation, medicaments; vitamins; mineral supplements; substances used for the treatment, prevention, diagnosis, cure or mitigation of disease or illness; or substances which affect the structure or function of the body; or

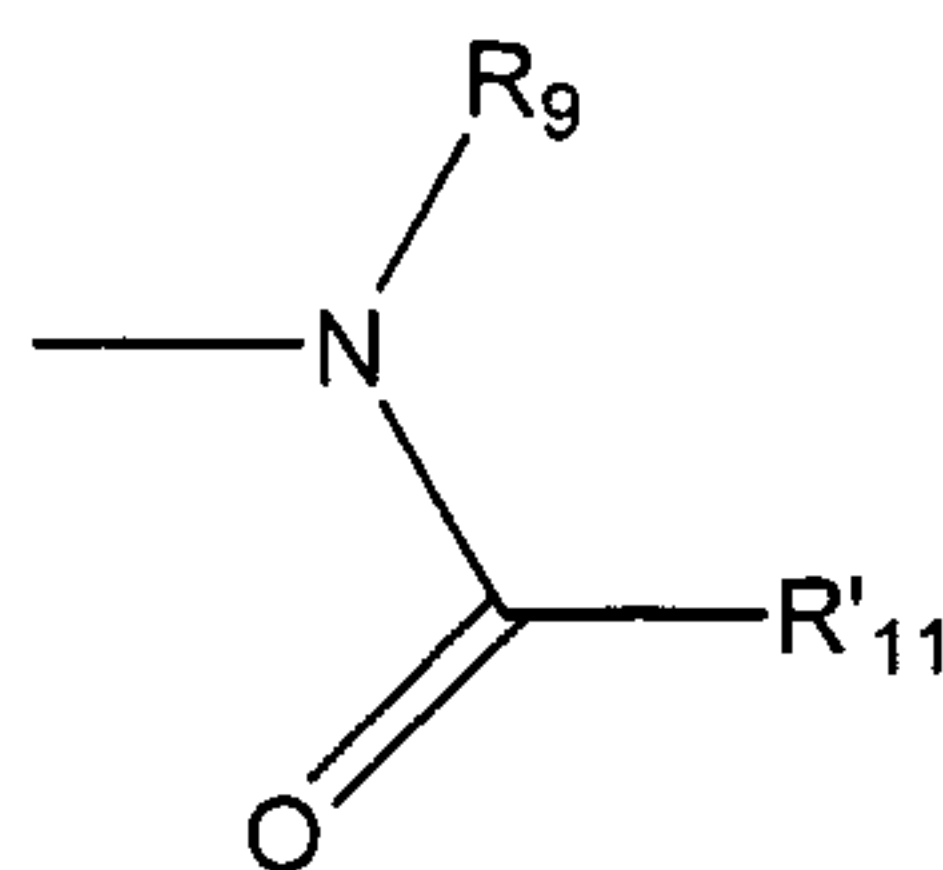
20 pro-drugs, which become biologically active or more active after they have been placed in a predetermined physiological environment.

The term "therapeutic index" refers to the therapeutic index of a drug defined as LD_{50}/ED_{50} .

'Acyl' refers to a group suitable for acylating a nitrogen atom to form an

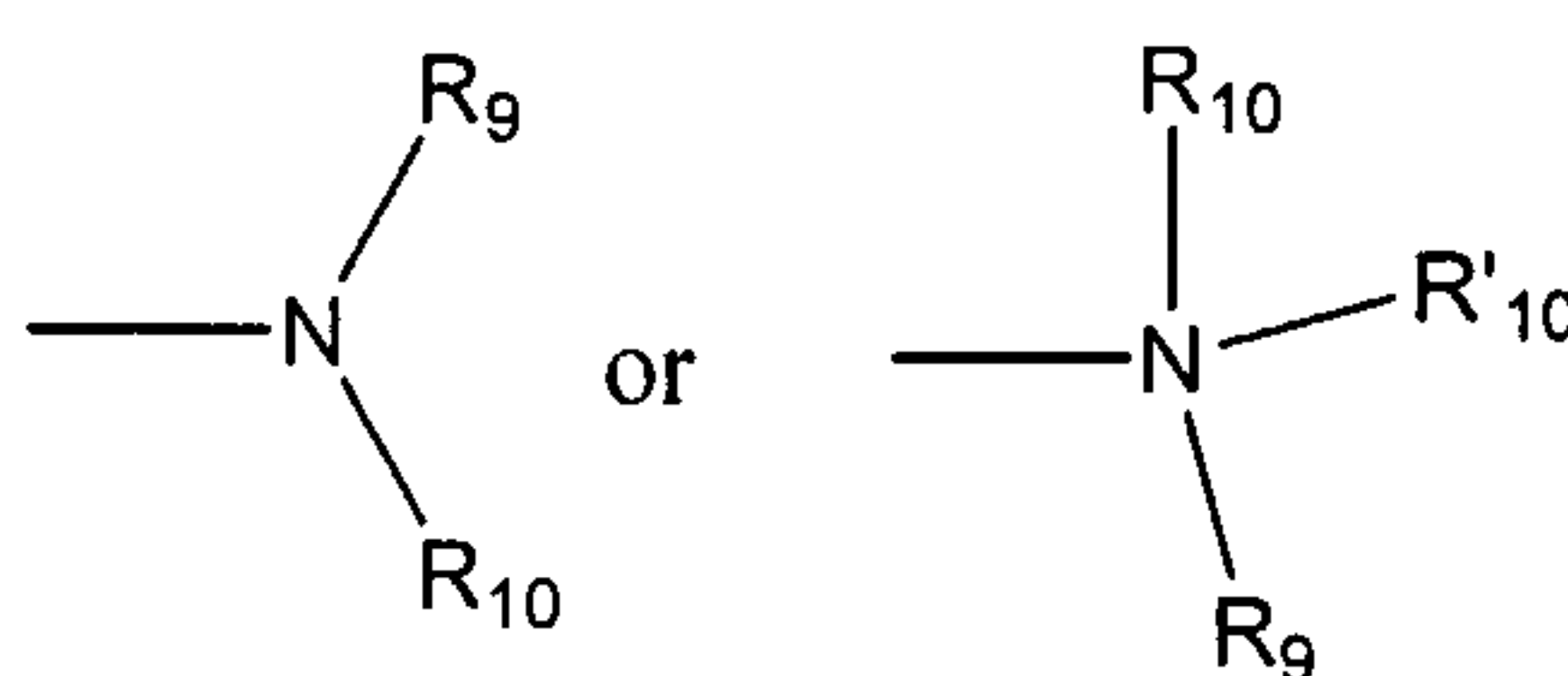
25 amide or carbamate, a carbon atom to form a ketone, a sulfur atom to form a thioester, or an oxygen atom to form an ester group, e.g., a hydrocarbon attached to a $-C(=O)-$ moiety. Preferred acyl groups include benzoyl, acetyl, tert-butyl acetyl, pivaloyl, and trifluoroacetyl. More preferred acyl groups include acetyl and benzoyl. The most preferred acyl group is acetyl.

The term 'acylamino' is art-recognized and preferably refers to a moiety that can be represented by the general formula:



wherein R_9 and R'_{11} each independently represent hydrogen or a hydrocarbon substituent, such as alkyl, heteroalkyl, aryl, heteroaryl, carbocyclic aliphatic, and heterocyclic aliphatic.

The terms 'amine' and 'amino' are art-recognized and refer to both unsubstituted and substituted amines as well as ammonium salts, e.g., as can be represented by the general formula:

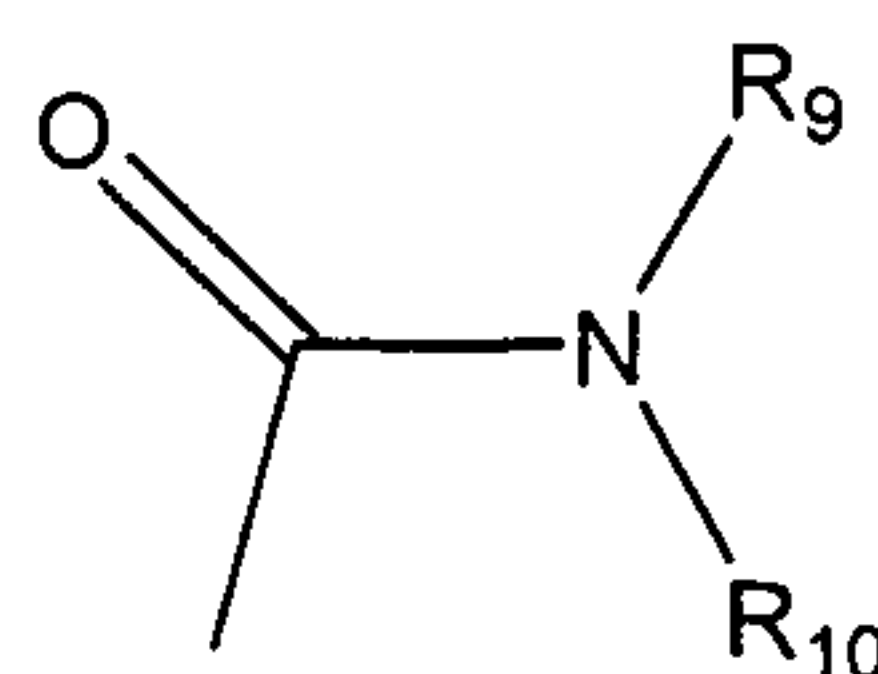


10

wherein R_9 , R_{10} , and R'_{10} each independently represent hydrogen or a hydrocarbon substituent, or R_9 and R_{10} taken together with the N atom to which they are attached complete a heterocycle having from 4 to 8 atoms in the ring structure. In preferred embodiments, none of R_9 , R_{10} , and R'_{10} is acyl, e.g., R_9 , R_{10} , and R'_{10} are selected from hydrogen, alkyl, heteroalkyl, aryl, heteroaryl, carbocyclic aliphatic, and heterocyclic aliphatic. The term 'alkylamine' as used herein means an amine group, as defined above, having at least one substituted or unsubstituted alkyl attached thereto. Amino groups that are positively charged (e.g., R'_{10} is present) are referred to as 'ammonium' groups. In amino groups other than ammonium groups, the amine is preferably basic, e.g., its conjugate acid has a pK_a above 7.

20

The terms 'amido' and 'amide' are art-recognized as an amino-substituted carbonyl, such as a moiety that can be represented by the general formula:



wherein R_9 and R_{10} are as defined above. In certain embodiments, the amide will include imides.

‘Alkyl’ refers to a saturated or unsaturated hydrocarbon chain having 1 to 18
 5 carbon atoms, preferably 1 to 12, more preferably 1 to 6, more preferably still 1 to 4 carbon atoms. Alkyl chains may be straight (e.g., *n*-butyl) or branched (e.g., *sec*-butyl, isobutyl, or *t*-butyl). Preferred branched alkyls have one or two branches, preferably one branch. Preferred alkyls are saturated. Unsaturated alkyls have one or more double bonds and/or one or more triple bonds. Preferred unsaturated alkyls
 10 have one or two double bonds or one triple bond, more preferably one double bond. Alkyl chains may be unsubstituted or substituted with from 1 to 4 substituents. Preferred alkyls are unsubstituted. Preferred substituted alkyls are mono-, di-, or trisubstituted. Preferred alkyl substituents include halo, haloalkyl, hydroxy, aryl (e.g., phenyl, tolyl, alkoxyphenyl, alkyloxycarbonylphenyl, halophenyl),
 15 heterocyclyl, and heteroaryl.

The terms ‘alkenyl’ and ‘alkynyl’ refer to unsaturated aliphatic groups analogous in length and possible substitution to the alkyls described above, but that contain at least one double or triple bond, respectively. When not otherwise indicated, the terms alkenyl and alkynyl preferably refer to lower alkenyl and lower
 20 alkynyl groups, respectively. When the term alkyl is present in a list with the terms alkenyl and alkynyl, the term alkyl refers to saturated alkyls exclusive of alkenyls and alkynyls.

The terms ‘alkoxyl’ and ‘alkoxy’ as used herein refer to an -O-alkyl group. Representative alkoxyl groups include methoxy, ethoxy, propyloxy, tert-butoxy, and
 25 the like. An ‘ether’ is two hydrocarbons covalently linked by an oxygen. Accordingly, the substituent of a hydrocarbon that renders that hydrocarbon an ether

can be an alkoxyl, or another moiety such as -O-aryl, -O-heteroaryl, -O-heteroalkyl, -O-aralkyl, -O-heteroaralkyl, -O-carbocyclic aliphatic, or -O-heterocyclic aliphatic.

The term 'alkylthio' refers to an -S-alkyl group. Representative alkylthio groups include methylthio, ethylthio, and the like. 'Thioether' refers to a sulfur atom
5 bound to two hydrocarbon substituents, e.g., an ether wherein the oxygen is replaced by sulfur. Thus, a thioether substituent on a carbon atom refers to a hydrocarbon-substituted sulfur atom substituent, such as alkylthio or arylthio, etc.

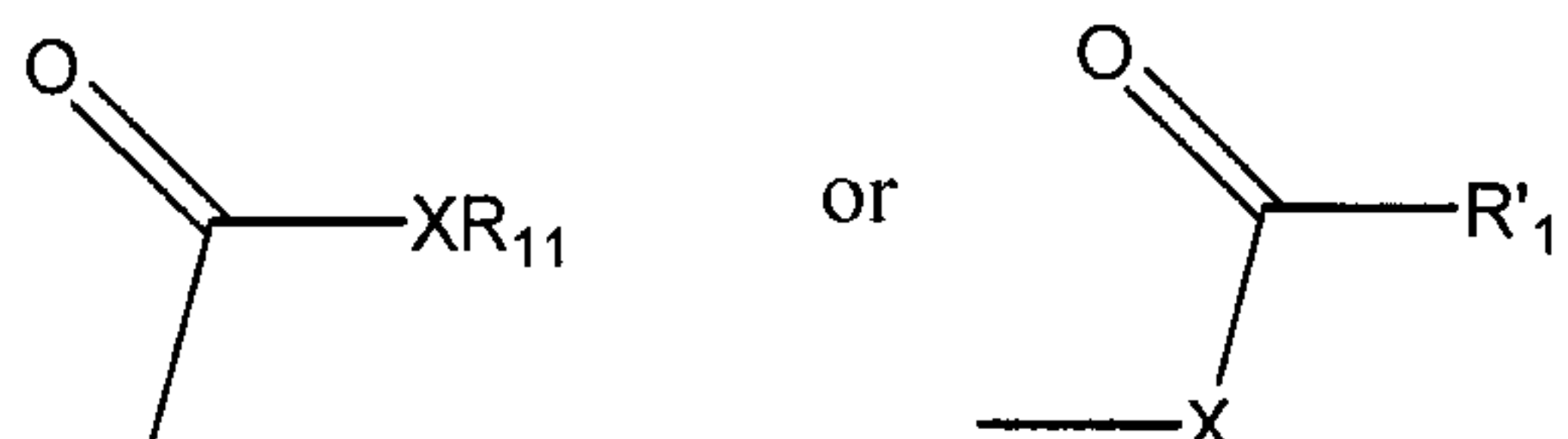
The term 'aralkyl', as used herein, refers to an alkyl group substituted with an aryl group.

10 'Aryl ring' refers to an aromatic hydrocarbon ring system. Aromatic rings are monocyclic or fused bicyclic ring systems, such as phenyl, naphthyl, etc. Monocyclic aromatic rings contain from about 5 to about 10 carbon atoms, preferably from 5 to 7 carbon atoms, and most preferably from 5 to 6 carbon atoms in the ring. Bicyclic aromatic rings contain from 8 to 12 carbon atoms, preferably 9 or 10 carbon atoms in
15 the ring. The term 'aryl' also includes bicyclic ring systems wherein only one of the rings is aromatic, e.g., the other ring is cycloalkyl, cycloalkenyl, or heterocyclyl. Aromatic rings may be unsubstituted or substituted with from 1 to about 5 substituents on the ring. Preferred aromatic ring substituents include: halo, cyano, lower alkyl, heteroalkyl, haloalkyl, phenyl, phenoxy, or any combination thereof.
20 More preferred substituents include lower alkyl, cyano, halo, and haloalkyl.

'Carbocyclic aliphatic ring' refers to a saturated or unsaturated hydrocarbon ring. Carbocyclic aliphatic rings are not aromatic. Carbocyclic aliphatic rings are monocyclic, or are fused, spiro, or bridged bicyclic ring systems. Monocyclic carbocyclic aliphatic rings contain from about 4 to about 10 carbon atoms, preferably
25 from 4 to 7 carbon atoms, and most preferably from 5 to 6 carbon atoms in the ring. Bicyclic carbocyclic aliphatic rings contain from 8 to 12 carbon atoms, preferably from 9 to 10 carbon atoms in the ring. Carbocyclic aliphatic rings may be unsubstituted or substituted with from 1 to 4 substituents on the ring. Preferred carbocyclic aliphatic ring substituents include halo, cyano, alkyl, heteroalkyl,

haloalkyl, phenyl, phenoxy or any combination thereof. More preferred substituents include halo and haloalkyl. Preferred carbocyclic aliphatic rings include cyclopentyl, cyclohexyl, cyclohexenyl, cycloheptyl, and cyclooctyl. More preferred carbocyclic aliphatic rings include cyclohexyl, cycloheptyl, and cyclooctyl.

- 5 The term 'carbonyl' is art-recognized and includes such moieties as can be represented by the general formula:



- wherein X is a bond or represents an oxygen or a sulfur, and R₁₁ represents a hydrogen, hydrocarbon substituent, or a pharmaceutically acceptable salt, R₁₁,
 10 represents a hydrogen or hydrocarbon substituent. Where X is an oxygen and R₁₁ or R₁₁' is not hydrogen, the formula represents an 'ester'. Where X is an oxygen, and R₁₁ is as defined above, the moiety is referred to herein as a carboxyl group, and particularly when R₁₁ is a hydrogen, the formula represents a 'carboxylic acid'.
 Where X is an oxygen, and R₁₁' is hydrogen, the formula represents a 'formate'. In
 15 general, where the oxygen atom of the above formula is replaced by sulfur, the formula represents a 'thiocarbonyl' group. Where X is a sulfur and R₁₁ or R₁₁' is not hydrogen, the formula represents a 'thioester.' Where X is a sulfur and R₁₁ is hydrogen, the formula represents a 'thiocarboxylic acid.' Where X is a sulfur and R₁₁' is hydrogen, the formula represents a 'thioformate.' On the other hand, where X
 20 is a bond, R₁₁ is not hydrogen, and the carbonyl is bound to a hydrocarbon, the above formula represents a 'ketone' group. Where X is a bond, R₁₁ is hydrogen, and the carbonyl is bound to a hydrocarbon, the above formula represents an 'aldehyde' or 'formyl' group.

- 'Ci alkyl' is an alkyl chain having i member atoms. For example, C4 alkyls
 25 contain four carbon member atoms. C4 alkyls containing may be saturated or unsaturated with one or two double bonds (cis or trans) or one triple bond. Preferred C4 alkyls are saturated. Preferred unsaturated C4 alkyl have one double bond. C4

alkyl may be unsubstituted or substituted with one or two substituents. Preferred substituents include lower alkyl, lower heteroalkyl, cyano, halo, and haloalkyl.

'Halogen' refers to fluoro, chloro, bromo, or iodo substituents. Preferred halo are fluoro, chloro and bromo; more preferred are chloro and fluoro.

5 'Haloalkyl' refers to a straight, branched, or cyclic hydrocarbon substituted with one or more halo substituents. Preferred haloalkyl are C1-C12; more preferred are C1-C6; more preferred still are C1-C3. Preferred halo substituents are fluoro and chloro. The most preferred haloalkyl is trifluoromethyl.

10 'Heteroalkyl' is a saturated or unsaturated chain of carbon atoms and at least one heteroatom, wherein no two heteroatoms are adjacent. Heteroalkyl chains contain from 1 to 18 member atoms (carbon and heteroatoms) in the chain, preferably 1 to 12, more preferably 1 to 6, more preferably still 1 to 4. Heteroalkyl chains may be straight or branched. Preferred branched heteroalkyl have one or two branches, preferably one branch. Preferred heteroalkyl are saturated. Unsaturated
15 heteroalkyl have one or more double bonds and/or one or more triple bonds. Preferred unsaturated heteroalkyl have one or two double bonds or one triple bond, more preferably one double bond. Heteroalkyl chains may be unsubstituted or substituted with from 1 to about 4 substituents unless otherwise specified. Preferred heteroalkyl are unsubstituted. Preferred heteroalkyl substituents include halo, aryl (e.g., phenyl,
20 tolyl, alkoxyphenyl, alkoxycarbonylphenyl, halophenyl), heterocyclyl, heteroaryl. For example, alkyl chains substituted with the following substituents are heteroalkyl: alkoxy (e.g., methoxy, ethoxy, propoxy, butoxy, pentoxy), aryloxy (e.g., phenoxy, chlorophenoxy, tolyloxy, methoxyphenoxy, benzyloxy, alkoxycarbonylphenoxy, acyloxyphenoxy), acyloxy (e.g., propionyloxy, benzoyloxy, acetoxy), carbamoyloxy,
25 carboxy, mercapto, alkylthio, acylthio, arylthio (e.g., phenylthio, chlorophenylthio, alkylphenylthio, alkoxyphenylthio, benzylthio, alkoxycarbonylphenylthio), amino (e.g., amino, mono- and di-C1-C3 alkylamino, methylphenylamino, methylbenzylamino, C1-C3 alkylamido, carbamamido, ureido, guanidino).

'Heteroatom' refers to a multivalent non-carbon atom, such as a boron, phosphorous, silicon, nitrogen, sulfur, or oxygen atom, preferably a nitrogen, sulfur, or oxygen atom. Groups containing more than one heteroatom may contain different heteroatoms.

5 'Heteroaryl ring' refers to an aromatic ring system containing carbon and from 1 to about 4 heteroatoms in the ring. Heteroaromatic rings are monocyclic or fused bicyclic ring systems. Monocyclic heteroaromatic rings contain from about 5 to about 10 member atoms (carbon and heteroatoms), preferably from 5 to 7, and most preferably from 5 to 6 in the ring. Bicyclic heteroaromatic rings contain from 8
10 to 12 member atoms, preferably 9 or 10 member atoms in the ring. The term 'heteroaryl' also includes bicyclic ring systems wherein only one of the rings is aromatic, e.g., the other ring is cycloalkyl, cycloalkenyl, or heterocyclyl. Heteroaromatic rings may be unsubstituted or substituted with from 1 to about 4 substituents on the ring. Preferred heteroaromatic ring substituents include halo,
15 cyano, lower alkyl, heteroalkyl, haloalkyl, phenyl, phenoxy or any combination thereof. Preferred heteroaromatic rings include thienyl, thiazolyl, oxazolyl, pyrrolyl, purinyl, pyrimidyl, pyridyl, and furanyl. More preferred heteroaromatic rings include thienyl, furanyl, and pyridyl.

 'Heterocyclic aliphatic ring' is a non-aromatic saturated or unsaturated ring
20 containing carbon and from 1 to about 4 heteroatoms in the ring, wherein no two heteroatoms are adjacent in the ring and preferably no carbon in the ring attached to a heteroatom also has a hydroxyl, amino, or thiol group attached to it. Heterocyclic aliphatic rings are monocyclic, or are fused or bridged bicyclic ring systems. Monocyclic heterocyclic aliphatic rings contain from about 4 to about 10 member
25 atoms (carbon and heteroatoms), preferably from 4 to 7, and most preferably from 5 to 6 member atoms in the ring. Bicyclic heterocyclic aliphatic rings contain from 8 to 12 member atoms, preferably 9 or 10 member atoms in the ring. Heterocyclic aliphatic rings may be unsubstituted or substituted with from 1 to about 4 substituents on the ring. Preferred heterocyclic aliphatic ring substituents include
30 halo, cyano, lower alkyl, heteroalkyl, haloalkyl, phenyl, phenoxy or any combination

thereof. More preferred substituents include halo and haloalkyl. Heterocyclyl groups include, for example, thiophene, thianthrene, furan, pyran, isobenzofuran, chromene, xanthene, phenoxathin, pyrrole, imidazole, pyrazole, isothiazole, isoxazole, pyridine, pyrazine, pyrimidine, pyridazine, indolizine, isoindole, indole, indazole, purine, 5 quinolizine, isoquinoline, hydantoin, oxazoline, imidazolinetrione, triazolinone, quinoline, phthalazine, naphthyridine, quinoxaline, quinazoline, quinoline, pteridine, carbazole, carboline, phenanthridine, acridine, phenanthroline, phenazine, phenarsazine, phenothiazine, furazan, phenoxazine, pyrrolidine, oxolane, thiolane, oxazole, piperidine, piperazine, morpholine, lactones, lactams such as azetidinones 10 and pyrrolidinones, sultams, sultones, and the like. Preferred heterocyclic aliphatic rings include piperazyl, morpholinyl, tetrahydrofuranyl, tetrahydropyranyl and piperidyl. Heterocycles can also be polycycles.

The term 'hydroxyl' means -OH.

'Lower alkyl' refers to an alkyl chain comprised of 1 to 5, preferably 1 to 4 15 carbon member atoms, more preferably 1 or 2 carbon member atoms. Lower alkyls may be saturated or unsaturated. Preferred lower alkyls are saturated. Lower alkyls may be unsubstituted or substituted with one or about two substituents. Preferred substituents on lower alkyl include cyano, halo, trifluoromethyl, amino, and hydroxyl. Throughout the application, preferred alkyl groups are lower alkyls. In 20 preferred embodiments, a substituent designated herein as alkyl is a lower alkyl. Likewise, 'lower alkenyl' and 'lower alkynyl' have similar chain lengths.

'Lower heteroalkyl' refers to a heteroalkyl chain comprised of 1 to 4, preferably 1 to 3 member atoms, more preferably 1 to 2 member atoms. Lower heteroalkyl contain one or two non-adjacent heteroatom member atoms. Preferred 25 lower heteroalkyl contain one heteroatom member atom. Lower heteroalkyl may be saturated or unsaturated. Preferred lower heteroalkyl are saturated. Lower heteroalkyl may be unsubstituted or substituted with one or about two substituents. Preferred substituents on lower heteroalkyl include cyano, halo, trifluoromethyl, and hydroxyl.

‘Mi heteroalkyl’ is a heteroalkyl chain having i member atoms. For example, M4 heteroalkyls contain one or two non-adjacent heteroatom member atoms. M4 heteroalkyls containing 1 heteroatom member atom may be saturated or unsaturated with one double bond (cis or trans) or one triple bond. Preferred M4 heteroalkyl
5 containing 2 heteroatom member atoms are saturated. Preferred unsaturated M4 heteroalkyl have one double bond. M4 heteroalkyl may be unsubstituted or substituted with one or two substituents. Preferred substituents include lower alkyl, lower heteroalkyl, cyano, halo, and haloalkyl.

‘Isocyanate’ refers to the group –NCO.

10 ‘Member atom’ refers to a polyvalent atom (e.g., C, O, N, or S atom) in a chain or ring system that constitutes a part of the chain or ring. For example, in cresol, six carbon atoms are member atoms of the ring and the oxygen atom and the carbon atom of the methyl substituent are not member atoms of the ring.

As used herein, the term ‘nitro’ means –NO₂.

15 ‘Pharmaceutically acceptable salt’ refers to a cationic salt formed at any acidic (e.g., hydroxamic or carboxylic acid) group, or an anionic salt formed at any basic (e.g., amino or guanidino) group. Such salts are well known in the art. See e.g., World Patent Publication 87/05297, Johnston et al., published September 11, 1987, incorporated herein by reference. Such salts are made by methods known to one of
20 ordinary skill in the art. It is recognized that the skilled artisan may prefer one salt over another for improved solubility, stability, formulation ease, price and the like. Determination and optimization of such salts is within the purview of the skilled artisan's practice. Preferred cations include the alkali metals (such as sodium and potassium), and alkaline earth metals (such as magnesium and calcium) and organic
25 cations, such as trimethylammonium, tetrabutylammonium, etc. Preferred anions include halides (such as chloride), sulfonates, carboxylates, phosphates, and the like. Clearly contemplated in such salts are addition salts that may provide an optical center where once there was none. For example, a chiral tartrate salt may be prepared from the compounds of the invention. This definition includes such chiral salts.

'Phenyl' is a six-membered monocyclic aromatic ring that may or may not be substituted with from 1 to 5 substituents. The substituents may be located at the ortho, meta or para position on the phenyl ring, or any combination thereof.

Preferred phenyl substituents include: halo, cyano, lower alkyl, heteroalkyl, haloalkyl, phenyl, phenoxy or any combination thereof. More preferred substituents on the phenyl ring include halo and haloalkyl. The most preferred substituent is halo.

The terms 'polycyclyl' and 'polycyclic group' refer to two or more rings (e.g., cycloalkyls, cycloalkenyls, heteroaryls, aryls and/or heterocyclyls) in which two or more member atoms of one ring are member atoms of a second ring. Rings that are joined through non-adjacent atoms are termed 'bridged' rings, and rings that are joined through adjacent atoms are 'fused rings'.

The term 'small organic molecule' refers to an organic compound of less than about 2500 amu, preferably less than 1500 amu. The term encompasses most pharmaceuticals that are not proteins or nucleic acids.

The term 'sulfhydryl' means $-SH$, and the term 'sulfonyl' means $-SO_2-$.

A 'substitution' or 'substituent' on a small organic molecule generally refers to a position on a multi-valent atom bound to a moiety other than hydrogen, e.g., a position on a chain or ring exclusive of the member atoms of the chain or ring. Such moieties include those defined herein and others as are known in the art, for example, halogen, alkyl, alkenyl, alkynyl, azide, haloalkyl, hydroxyl, carbonyl (such as carboxyl, alkoxycarbonyl, formyl, ketone, or acyl), thiocarbonyl (such as thioester, thioacetate, or thioformate), alkoxy, phosphoryl, phosphonate, phosphinate, amine, amide, amidine, imine, cyano, nitro, azido, sulfhydryl, alkylthio, sulfate, sulfonate, sulfamoyl, sulfonamido, sulfonyl, silyl, ether, cycloalkyl, heterocyclyl, heteroalkyl, heteroalkenyl, and heteroalkynyl, heteroaralkyl, aralkyl, aryl or heteroaryl. It will be understood by those skilled in the art that certain substituents, such as aryl, heteroaryl, polycyclyl, alkoxy, alkylamino, alkyl, cycloalkyl, heterocyclyl, alkenyl, alkynyl, heteroalkyl, heteroalkenyl, and heteroalkynyl, can themselves be substituted, if appropriate. This invention is not

intended to be limited in any manner by the permissible substituents of organic compounds. It will be understood that 'substitution' or 'substituted with' includes the implicit proviso that such substitution is in accordance with permitted valence of the substituted atom and the substituent, and that the substitution results in a stable
5 compound, e.g., which does not spontaneously undergo transformation such as by rearrangement, cyclization, elimination, hydrolysis, etc.

As used herein, the definition of each expression, e.g., alkyl, m, n, etc., when it occurs more than once in any structure, is intended to be independent of its definition elsewhere in the same structure.

10 The abbreviations Me, Et, Ph, Tf, Nf, Ts, and Ms represent methyl, ethyl, phenyl, trifluoromethanesulfonyl, nonafluorobutanesulfonyl, *p*-toluenesulfonyl, and methanesulfonyl, respectively. A more comprehensive list of the abbreviations utilized by organic chemists of ordinary skill in the art appears in the first issue of each volume of the *Journal of Organic Chemistry*; this list is typically presented in a
15 table entitled Standard List of Abbreviations. The abbreviations contained in said list, and all abbreviations utilized by organic chemists of ordinary skill in the art are hereby incorporated by reference.

The terms *ortho*, *meta* and *para* apply to 1,2-, 1,3- and 1,4-disubstituted benzenes, respectively. For example, the names 1,2-dimethylbenzene and *ortho*-
20 dimethylbenzene are synonymous.

The terms triflyl, tosyl, mesyl, and nonafllyl are art-recognized and refer to trifluoromethanesulfonyl, *p*-toluenesulfonyl, methanesulfonyl, and nonafluorobutanesulfonyl groups, respectively. The terms triflate, tosylate, mesylate, and nonaflate are art-recognized and refer to trifluoromethanesulfonate ester, *p*-
25 toluenesulfonate ester, methanesulfonate ester, and nonafluorobutanesulfonate ester functional groups and molecules that contain said groups, respectively.

The phrase 'protecting group' as used herein means temporary substituents that protect a potentially reactive functional group from undesired chemical transformations. Examples of such protecting groups include esters of carboxylic

acids, silyl ethers of alcohols, and acetals and ketals of aldehydes and ketones, respectively. The field of protecting group chemistry has been reviewed (Greene, T.W.; Wuts, P.G.M. *Protective Groups in Organic Synthesis*, 2nd ed.; Wiley: New York, 1991; and Kocienski, P.J. *Protecting Groups*, Georg Thieme Verlag: New York, 1994).

The term 'prodrug' is intended to encompass compounds that, under physiological conditions, are converted into the therapeutically active agents of the present invention. A common method for making a prodrug is to include selected moieties, such as esters or ketals, that are hydrolyzed under physiological conditions to reveal the desired molecule. In other embodiments, the prodrug is converted by an enzymatic activity of the host animal.

For purposes of this invention, the chemical elements are identified in accordance with the Periodic Table of the Elements, CAS version, Handbook of Chemistry and Physics, 67th Ed., 1986-87, inside cover. Also for purposes of this invention, the term 'hydrocarbon' is contemplated to include all permissible compounds or moieties having at least one carbon-hydrogen bond. In a broad aspect, the permissible hydrocarbons include acyclic and cyclic, branched and unbranched, carbocyclic and heterocyclic, aromatic and nonaromatic organic compounds which can be substituted or unsubstituted.

Contemplated equivalents of the compounds described above include compounds which otherwise correspond thereto, and which have the same useful properties thereof, wherein one or more simple variations of substituents are made which do not adversely affect the efficacy of the compound. In general, the compounds of the present invention may be prepared by the methods illustrated in the general reaction schemes as, for example, described below, or by modifications thereof, using readily available starting materials, reagents and conventional synthesis procedures. In these reactions, it is also possible to make use of variants that are in themselves known, but are not mentioned here.

III. Exemplary Applications of Methods and Compositions

Therapeutic compositions according to the invention contain a therapeutic agent and a material of the invention, such as a cyclodextrin-based material. The therapeutic agent may be any synthetic or naturally occurring biologically active therapeutic agent including those known in the art. Examples of suitable therapeutic agents include, but are not limited to, antibiotics, steroids, polynucleotides (e.g., genomic DNA, cDNA, mRNA and antisense oligonucleotides), plasmids, proteins, polypeptides, peptide fragments, small molecules (e.g., doxorubicin) and other biologically active macromolecules such as, for example, proteins and enzymes. In certain embodiments, the agent may be associated with a delivery system, e.g., a nucleic acid may be contained in a virus, or an agent may be carried within liposomes or microspheres, and the delivery system is dispersed through the material.

A therapeutic composition of the invention may be prepared by means known in the art. In a preferred embodiment, a material of the invention, such as a cyclodextrin-based material, is mixed with or prepared in the presence of a therapeutic agent, as described above. According to the invention, the material acts as a delivery vehicle for the therapeutic agent. The therapeutic agent (and/or an adjuvant) and material may associate by means recognized by those of skill in the art such as, for example, electrostatic interaction, hydrogen bonding, hydrophobic interaction, formation of inclusion complexes with the inclusion hosts, or covalent attachment to the polymer, preferably by a reversible attachment such as an ester or carbonate. In certain embodiments, the therapeutic agent and/or adjuvant may be covalently attached, optionally through a reversible linkage, to a moiety that forms an inclusion complex with the inclusion hosts, e.g., cyclodextrin. The degree of association may be determined by techniques known in the art including, for example, fluorescence studies, DNA mobility studies, light scattering, electron microscopy, and will vary depending upon the therapeutic agent. As a mode of delivery, for example, a therapeutic composition of the invention containing a material of the invention and DNA may be used to aid in transfection, i.e., the uptake of DNA into an animal (e.g., human) cell. (Boussif, O. Proceedings of the National

Academy of Sciences, 92:7297-7301(1995); Zanta et al. Bioconjugate Chemistry, 8:839-844 (1997)).

In certain embodiments, a therapeutic composition of the invention is in a form suitable for injection, and in other embodiments, the composition is suitable for
5 topical application. Other modes of administration of a therapeutic composition of the invention include, depending on the state of the therapeutic composition, methods known in the art such as, but not limited to, oral administration, parenteral, intravenous, intranasal, intraocular, intracranial or intraperitoneal injection.

Depending upon the type of therapeutic agent used, a therapeutic
10 composition of the invention may be used in a variety of therapeutic methods (e.g. DNA vaccines, antibiotics, antiviral agents) for the treatment of inherited or acquired disorders such as, for example, cystic fibrosis, Gaucher's disease, muscular dystrophy, AIDS, cancers (e.g., multiple myeloma, leukemia, melanoma, and ovarian carcinoma), cardiovascular conditions (e.g., progressive heart failure, restenosis, and
15 hemophilia), and neurological conditions (e.g., brain trauma). In other embodiments, subject compositions can be used in the treatment of wounds, such as incisions, diabetic ulcers, bedsores, lacerations, burns, etc.

The therapeutic agent may range from a nucleic acid (such as a vector, an RNAi construct, or an antisense oligonucleotide) or protein to a small organic
20 molecule. In certain embodiments, the agent is an anti-cancer (such as camptothecin or related derivatives), anti-fungal, anti-bacterial, anti-mycotic, or anti-viral therapeutic. In certain embodiments, the agent is a receptor agonist. In certain embodiments, the agent is a receptor antagonist. In certain embodiments, the therapeutic agent is a protease inhibitor. Furthermore, a polymer of the present
25 invention may contain one kind of therapeutic agent, or may contain more than one kind of therapeutic agent. For instance, two or more different cancer drugs, or a cancer drug and an immunosuppressant, or an antibiotic and an anti-inflammatory agent may be included in the composition.

Depending upon the type of therapeutic agent used, a therapeutic composition of the invention may be used in a variety of therapeutic methods (e.g. DNA vaccines, antibiotics, antiviral agents) for the treatment of inherited or acquired disorders such as, for example, cystic fibrosis, Gaucher's disease, muscular
5 dystrophy, AIDS, cancers (e.g., multiple myeloma, leukemia, melanoma, and ovarian carcinoma), cardiovascular conditions (e.g., progressive heart failure, restenosis, and hemophilia), and neurological conditions (e.g., brain trauma).

In certain particular embodiments, compositions of the invention may be used to treat wounds (i.e., to promote wound healing. Although the matrix alone may
10 be useful as a wound sealant, such compositions may include, for example, PDGF-B or an expression vector for producing PDGF-B in a target cell, stimulators of cell proliferation or differentiation, stem cells or progenitor cells, and/or other compounds known to be effective in promoting healing, inhibiting infection, etc.

In other embodiments, compositions of the invention may be used in the
15 treatment of cancer. Such compositions may include a chemotherapeutic agent, an angiogenesis-inhibiting agent, a cell proliferation inhibitor, a radiosensitizer, and/or any other agent useful in the treatment of cancer.

For example, compounds that may be formulated in a subject composition for the treatment of cancer include: aminoglutethimide, amsacrine, anastrozole,
20 asparaginase, bcg, bicalutamide, bleomycin, buserelin, busulfan, campothecin, capecitabine, carboplatin, carmustine, chlorambucil, cisplatin, cladribine, clodronate, colchicine, cyclophosphamide, cyproterone, cytarabine, dacarbazine, dactinomycin, daunorubicin, dienestrol, diethylstilbestrol, docetaxel, doxorubicin, epirubicin, estradiol, estramustine, etoposide, exemestane, filgrastim, fludarabine,
25 fludrocortisone, fluorouracil, fluoxymesterone, flutamide, gemcitabine, genistein, goserelin, hydroxyurea, idarubicin, ifosfamide, imatinib, interferon, irinotecan, ironotecan, letrozole, leucovorin, leuprolide, levamisole, lomustine, mechlorethamine, medroxyprogesterone, megestrol, melphalan, mercaptopurine, mesna, methotrexate, mitomycin, mitotane, mitoxantrone, nilutamide, nocodazole,
30 octreotide, oxaliplatin, paclitaxel, pamidronate, pentostatin, plicamycin, porfimer,

procarbazine, raltitrexed, rituximab, streptozocin, suramin, tamoxifen, temozolomide, teniposide, testosterone, thioguanine, thiotepa, titanocene dichloride, topotecan, trastuzumab, tretinoin, vinblastine, vincristine, vindesine, and vinorelbine.

- 5 These chemotherapeutic agents may be categorized by their mechanism of action into, for example, following groups: anti-metabolites/anti-cancer agents, such as pyrimidine analogs (5-fluorouracil, floxuridine, capecitabine, gemcitabine and cytarabine) and purine analogs, folate antagonists and related inhibitors (mercaptapurine, thioguanine, pentostatin and 2-chlorodeoxyadenosine (cladribine));
- 10 antiproliferative/antimitotic agents including natural products such as vinca alkaloids (vinblastine, vincristine, and vinorelbine), microtubule disruptors such as taxane (paclitaxel, docetaxel), vincristin, vinblastin, nocodazole, epothilones and navelbine, epidipodophyllotoxins (teniposide), DNA damaging agents (actinomycin, amsacrine, anthracyclines, bleomycin, busulfan, camptothecin, carboplatin, chlorambucil,
- 15 cisplatin, cyclophosphamide, cytoxan, dactinomycin, daunorubicin, doxorubicin, epirubicin, hexamethylmelamineoxaliplatin, iphosphamide, melphalan, merchlorhtamine, mitomycin, mitoxantrone, nitrosourea, plicamycin, procarbazine, teniposide, triethylenethiophosphoramidate and etoposide (VP16)); antibiotics such as dactinomycin (actinomycin D), daunorubicin, doxorubicin (adriamycin), idarubicin,
- 20 anthracyclines, mitoxantrone, bleomycins, plicamycin (mithramycin) and mitomycin; enzymes (L-asparaginase which systemically metabolizes L-asparagine and deprives cells which do not have the capacity to synthesize their own asparagine); antiplatelet agents; antiproliferative/antimitotic alkylating agents such as nitrogen mustards (mechlorethamine, cyclophosphamide and analogs, melphalan,
- 25 chlorambucil), ethylenimines and methylmelamines (hexamethylmelamine and thiotepa), alkyl sulfonates-busulfan, nitrosoureas (carmustine (BCNU) and analogs, streptozocin), trazenes - dacarbazine (DTIC); antiproliferative/antimitotic antimetabolites such as folic acid analogs (methotrexate); platinum coordination complexes (cisplatin, carboplatin), procarbazine, hydroxyurea, mitotane,
- 30 aminogluthimide; hormones, hormone analogs (estrogen, tamoxifen, goserelin, bicalutamide, nilutamide) and aromatase inhibitors (letrozole, anastrozole);

anticoagulants (heparin, synthetic heparin salts and other inhibitors of thrombin);
fibrinolytic agents (such as tissue plasminogen activator, streptokinase and
urokinase), aspirin, COX-2 inhibitors, dipyridamole, ticlopidine, clopidogrel,
abciximab; antimigratory agents; antisecretory agents (breveldin);
5 immunosuppressives (cyclosporine, tacrolimus (FK-506), sirolimus (rapamycin),
azathioprine, mycophenolate mofetil); anti-angiogenic compounds (TNP-470,
genistein) and growth factor inhibitors (vascular endothelial growth factor (VEGF)
inhibitors, fibroblast growth factor (FGF) inhibitors); angiotensin receptor blocker;
nitric oxide donors; anti-sense oligonucleotides; antibodies (trastuzumab); cell cycle
10 inhibitors and differentiation inducers (tretinoin); mTOR inhibitors, topoisomerase
inhibitors (doxorubicin (adriamycin), amsacrine, camptothecin, daunorubicin,
dactinomycin, eniposide, epirubicin, etoposide, idarubicin and mitoxantrone,
topotecan, irinotecan), corticosteroids (cortisone, dexamethasone, hydrocortisone,
methylprednisolone, prednisone, and prednisolone); growth factor signal transduction
15 kinase inhibitors; mitochondrial dysfunction inducers and caspase activators;
chromatin disruptors.

According to the invention, a method of treatment administers a
therapeutically effective amount of a therapeutic composition of the invention. A
therapeutically effective amount, as recognized by those of skill in the art, will be
20 determined on a case by case basis. Factors to be considered include, but are not
limited to, the disorder to be treated and the physical characteristics of the one
suffering from the disorder.

Another embodiment of the invention is a composition containing at least
one biologically active compound having agricultural utility and a linear
25 cyclodextrin-modified polymer or a linear oxidized cyclodextrin-modified polymer
of the invention. The agriculturally biologically active compounds include those
known in the art. For example, suitable agriculturally biologically active compounds
include, but are not limited to, fungicides, herbicides, insecticides, and mildewcides.

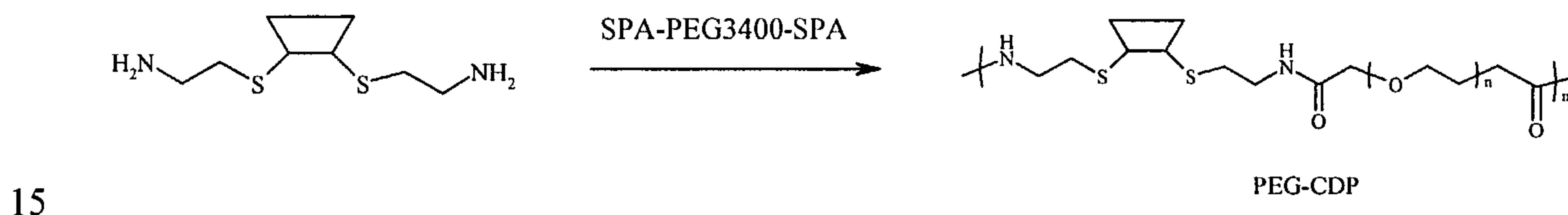
IV. Exemplary Compositions

In certain embodiments, the underlying polymers are linear cyclodextrin-containing polymers, e.g., the polymer backbone includes cyclodextrin moieties. For example, the polymer may be a water-soluble, linear cyclodextrin polymer produced by providing at least one cyclodextrin derivative modified to bear one reactive site at each of exactly two positions, and reacting the cyclodextrin derivative with a linker having exactly two reactive moieties capable of forming a covalent bond with the reactive sites under polymerization conditions that promote reaction of the reactive sites with the reactive moieties to form covalent bonds between the linker and the cyclodextrin derivative, whereby a linear polymer comprising alternating units of cyclodextrin derivatives and linkers is produced. A variety of suitable polymers are described in U.S. Patent Applications 20020151523 and 10/656,838. Alternatively the polymer may be a water-soluble, linear cyclodextrin polymer having a linear polymer backbone, which polymer comprises a plurality of substituted or unsubstituted cyclodextrin moieties and linker moieties in the linear polymer backbone, wherein each of the cyclodextrin moieties, other than a cyclodextrin moiety at the terminus of a polymer chain, is attached to two of said linker moieties, each linker moiety covalently linking two cyclodextrin moieties. In yet another embodiment, the polymer is a water-soluble, linear cyclodextrin polymer comprising a plurality of cyclodextrin moieties covalently linked together by a plurality of linker moieties, wherein each cyclodextrin moiety, other than a cyclodextrin moiety at the terminus of a polymer chain, is attached to two linker moieties to form a linear cyclodextrin polymer.

The linker group(s) may be an alkylene chain, a polyethylene glycol (PEG) chain, polysuccinic anhydride, poly-L-glutamic acid, poly(ethyleneimine), an oligosaccharide, an amino acid chain, or any other suitable linkage. In certain embodiments, the linker group itself can be stable under physiological conditions, such as an alkylene chain, or it can be cleavable under physiological conditions, such as by an enzyme (e.g., the linkage contains a peptide sequence that is a substrate for a peptidase), or by hydrolysis (e.g., the linkage contains a hydrolyzable group, such as an ester or thioester). The linker groups can be biologically inactive, such as a

PEG, polyglycolic acid, or polylactic acid chain, or can be biologically active, such as an oligo- or polypeptide that, when cleaved from the moieties, binds a receptor, deactivates an enzyme, etc. Various oligomeric linker groups that are biologically compatible and/or bioerodible are known in the art, and the selection of the linkage
 5 may influence the ultimate properties of the material, such as whether it is durable when implanted, whether it gradually deforms or shrinks after implantation, or whether it gradually degrades and is absorbed by the body. The linker group may be attached to the moieties by any suitable bond or functional group, including carbon-carbon bonds, esters, ethers, amides, amines, carbonates, carbamates, sulfonamides,
 10 etc.

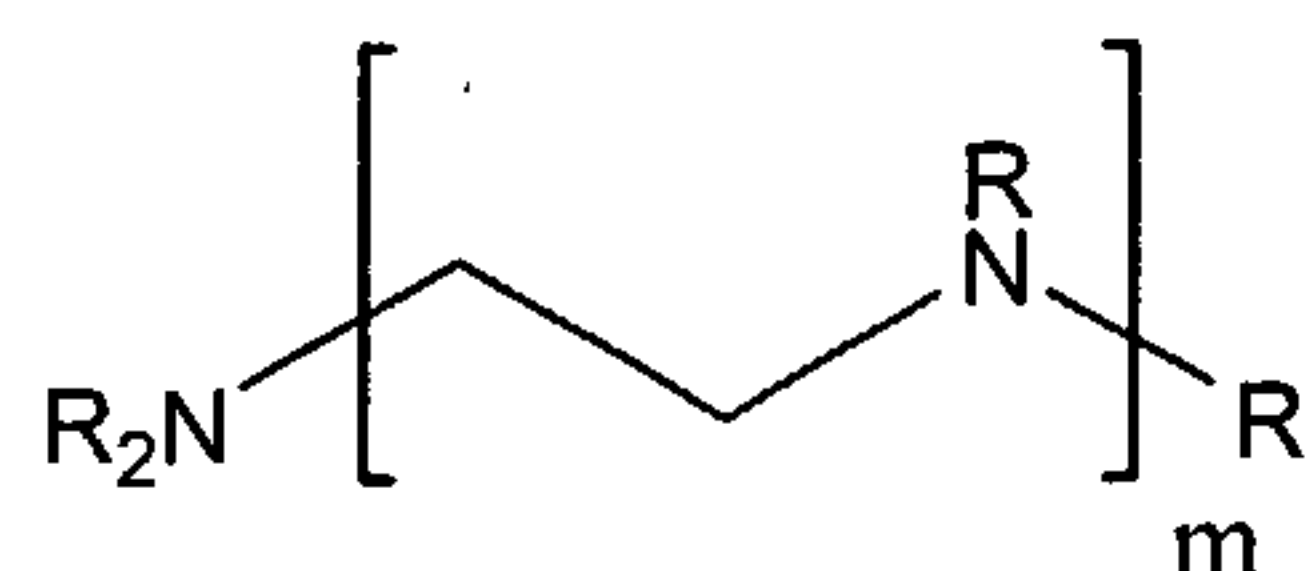
In exemplary embodiments, the cyclodextrin polymers used for forming the material are copolymers of cyclodextrin and polyethylene glycol (PEG). Such polymers can be prepared by techniques well known in the art, such as the reaction exemplified by the following equation:



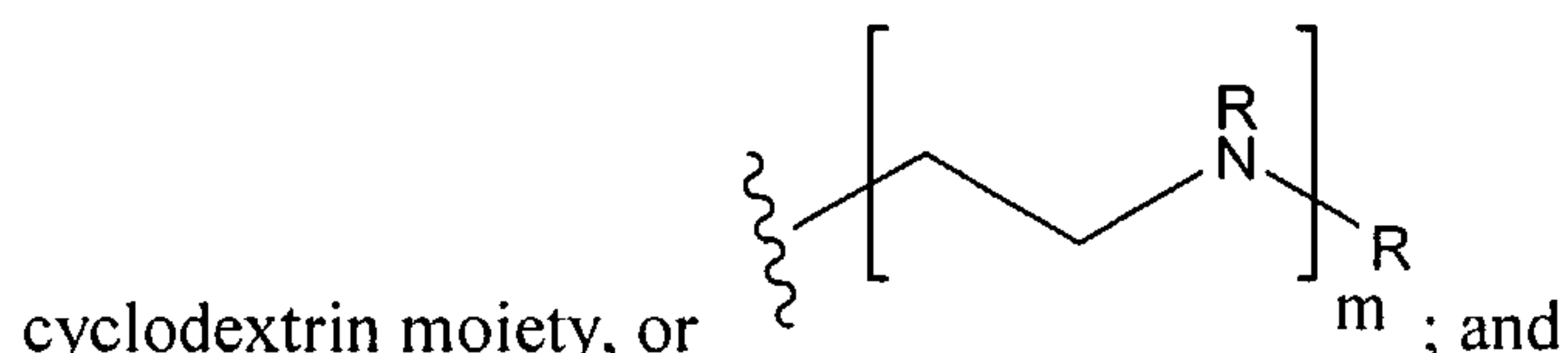
wherein the trapezoid represents a cyclodextrin moiety, as described in greater detail below, and n represents an integer from 1 to 20, preferably from 2 to 12. The polymers may be modified, e.g., by covalent attachment of therapeutic moieties, e.g.,
 20 through a linker that is cleavable under physiological conditions.

In such polymers, cyclodextrin moieties may represent at least 2% of the weight of the copolymer, preferably at least 5% or 10%, or even as much as 20%, 40%, 50%, 60%, 80%, or even 90% of the weight of the copolymer.

In certain embodiments, the cyclodextrin polymers used for forming the
 25 material have a structure of the formula:



wherein R represents, independently for each occurrence, H, lower alkyl, a



m, independently for each occurrence, represents an integer from 2-10,000, preferably from 10 to 5,000, or from 100 to 1,000. Suitable polymers of this type are discussed at greater length in U.S. Patent Application No. 10/372,723 and PCT Application WO 03/072637.

In certain embodiments, R represents a cyclodextrin moiety for at least about 1%, more preferably at least about 3%, and up to about 5%, 10%, 20%, 35%, or even 50%, of the nitrogen atoms that would be primary amines (i.e., bearing two occurrences of R that represent H) but for the cyclodextrin moieties.

In certain embodiments, the cyclodextrin moieties make up at least about 2%, 3%, or 4% by weight, up to 5%, 7%, or even 10% of the cyclodextrin-modified polymer by weight.

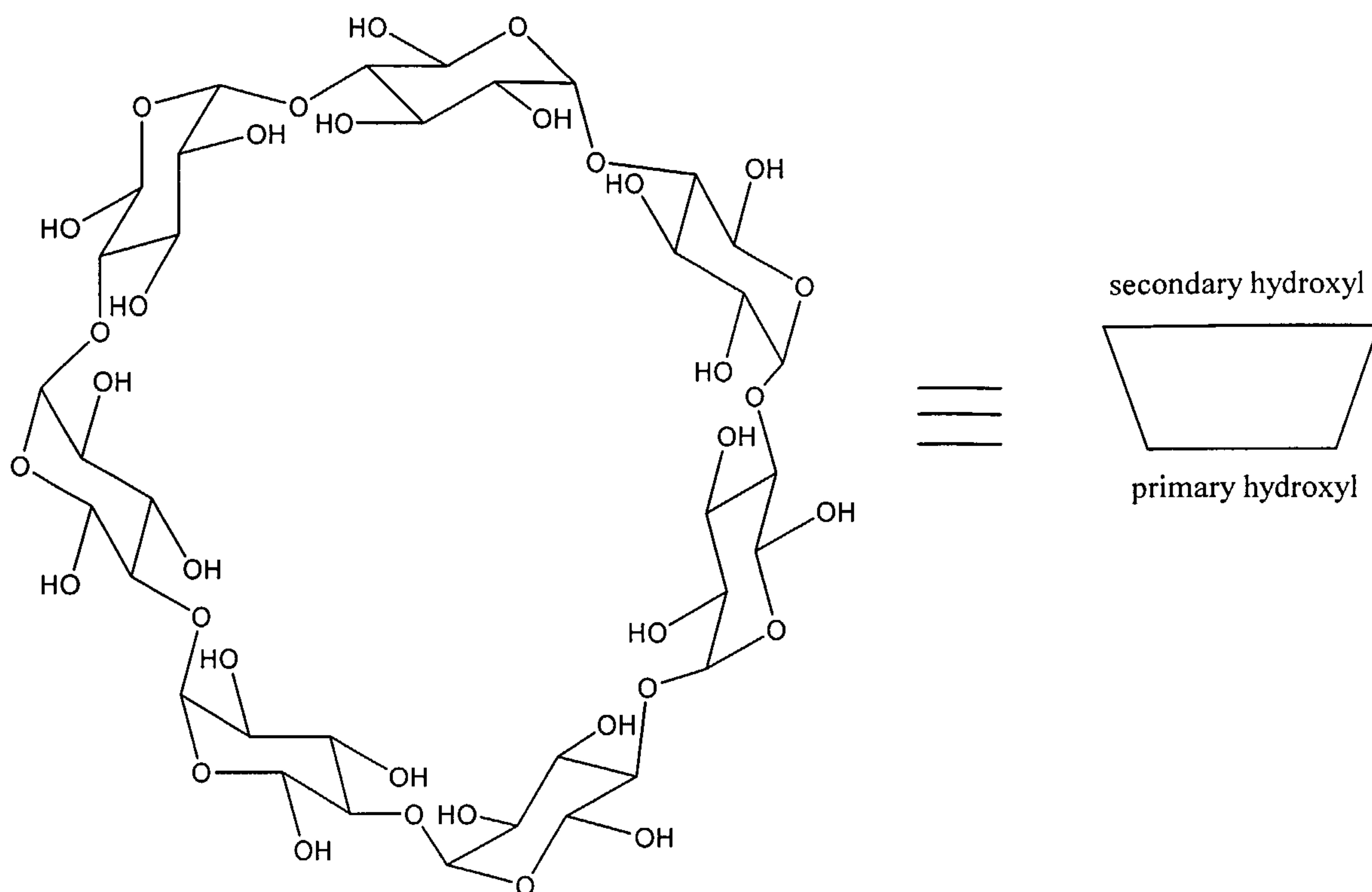
In certain embodiments, at least about 2%, 3%, or 4% by weight, up to 5%, 7%, or even 10% of the ethylenimine subunits in the polymer are modified with a cyclodextrin moiety.

Copolymers of poly(ethylenimine) that bear nucleophilic amino substituents susceptible to derivatization with cyclodextrin moieties can also be used to prepare cyclodextrin-modified polymers within the scope of the present invention.

Exemplary cyclodextrin moieties include cyclic structures consisting essentially of from 6 to 9 saccharide moieties, such as cyclodextrin and oxidized cyclodextrin. A cyclodextrin moiety optionally comprises a linker moiety that forms

a covalent linkage between the cyclic structure and the polymer backbone, preferably having from 1 to 20 atoms in the chain, such as alkyl chains, including dicarboxylic acid derivatives (such as glutaric acid derivatives, succinic acid derivatives, and the like), and heteroalkyl chains, such as oligoethylene glycol chains. Cyclodextrin
5 moieties may further include one or more carbohydrate moieties, preferably simple carbohydrate moieties such as galactose, attached to the cyclic core, either directly (i.e., via a carbohydrate linkage) or through a linker group.

Cyclodextrins are cyclic polysaccharides containing naturally occurring D-(+)-glucopyranose units in an α -(1,4) linkage. The most common cyclodextrins are
10 alpha ((α)-cyclodextrins, beta (β)-cyclodextrins and gamma (γ)-cyclodextrins which contain, respectively, six, seven, or eight glucopyranose units. Structurally, the cyclic nature of a cyclodextrin forms a torus or donut-like shape having an inner apolar or hydrophobic cavity, the secondary hydroxyl groups situated on one side of the cyclodextrin torus and the primary hydroxyl groups situated on the other. Thus,
15 using (β)-cyclodextrin as an example, a cyclodextrin is often represented schematically as follows.



The side on which the secondary hydroxyl groups are located has a wider diameter
 5 than the side on which the primary hydroxyl groups are located. The hydrophobic
 nature of the cyclodextrin inner cavity allows for the inclusion of a variety of
 compounds. (Comprehensive Supramolecular Chemistry, Volume 3, J.L. Atwood et
 al., eds., Pergamon Press (1996); T. Cserhati, Analytical Biochemistry, 225:328-
 332(1995); Husain et al., Applied Spectroscopy, 46:652-658 (1992); FR 2 665 169).
 10 Additional methods for modifying polymers are disclosed in Suh, J. and Noh, Y.,
Bioorg. Med. Chem. Lett. **1998**, 8, 1327-1330.

Cyclodextrins have been used as a delivery vehicle of various therapeutic
 compounds by forming inclusion complexes with various drugs that can fit into the
 hydrophobic cavity of the cyclodextrin or by forming non-covalent association
 15 complexes with other biologically active molecules such as oligonucleotides and
 derivatives thereof. For example, see U.S. Patents 4,727,064, 5,608,015, 5,276,088,
 and 5,691,316. Various cyclodextrin-containing polymers and methods of their

preparation are also known in the art. Comprehensive Supramolecular Chemistry, Volume 3, J.L. Atwood et al., eds., Pergamon Press (1996). Cyclodextrin polymers have been produced by linking or cross-linking cyclodextrins or mixtures of cyclodextrins and other carbohydrates with polymerizing agents, e.g. epichlorhydrin, diisocyanates, diepoxides (Insoluble cyclodextrin polymer beads, Chem. Abstr. No. 222444m, 102: 94; Zsador and Fenyvesi, 1st. Int. Symp. on Cyclodextrins, J. Szejtli, ed., D. Reidel Publishing Co., Boston, pp. 327-336; Fenyvesi et al., 1979, Ann. Univ. Budapest, Section Chim. 15: 13 22; and Wiedenhof et al., 1969, Die Stirke 21: 119-123). These polymerizing agents are capable of reacting with the primary and secondary hydroxy groups on carbons 6, 2, and 3. Cyclodextrin-modified polymer carriers can be coupled to biorecognition molecules for targeting the delivery of drugs to their site of action. See also U.S. Patent Nos. 6,180,739, 5,981,740, 5,929,131, 5,910, 551, and 5,792,821 (disclosing polymerizable cyclodextrin derivatives), 6,048,736 (discussing drug delivery using cyclodextrin polymers), (disclosing polymerizable cyclodextrin derivatives), 5,856,416 and 5,593,768 (disclosing monomers and polymers that bear cyclodextrin moieties), 5,608,015 (disclosing methods for preparing polymerizable cyclodextrin derivatives), and 5,516,766 (describing uses for cyclodextrin polymers).

The crosslinking molecules generally comprise two or more moieties that form inclusion complexes with cyclodextrin or another inclusion host, the moieties being covalently linked by a chain of atoms that allows the moieties to be spaced from 0.5 to 50 nm apart, preferably 1 to 30 nm apart. The moieties can be selected from any molecules that form inclusion complexes with an inclusion host such as cyclodextrin, e.g., phenyl rings, adamantane polycycles, cholesterol, naphthol derivatives, etc. See, for example, Szejtli, *Cyclodextrins and Their Inclusion Complexes*; Akademiai Klado, Budapest, 1982; and Bender et al., *Cyclodextrin Chemistry*, Springer-Verlag, Berlin, 1978. Cyclodextrins are able to form inclusion complexes with an array of organic molecules including, for example, drugs, pesticides, and herbicides. See, Tenjarla et al., *J. Pharm. Sci.*, 87: 425-429 (1998); Zughul et al., *Pharm. Dev. Technol.*, 3: 43-53 (1998); and Albers et al., *Crit. Rev. Ther. Drug Carrier Syst.*, 12: 311-337 (1995). The moieties in a crosslinking

molecule may be the same or different, and different crosslinking molecules may be used simultaneously in a single material.

The covalent linkage between the moieties may be any suitable linkage, such as an alkylene chain, a polyethylene glycol (PEG) chain, poly(ethyleneimine), an oligosaccharide, an amino acid chain, or any other suitable linkage. The linkage can be stable under physiological conditions, such as an alkylene chain, or it can be cleavable under physiological conditions, such as by an enzyme (e.g., the linkage contains a peptide sequence that is a substrate for a peptidase), or by hydrolysis (e.g., the linkage contains a hydrolyzable group, such as an ester or thioester). The linkage can be biologically inactive, such as a PEG, polyglycolic acid, or polylactic acid chain, or can be biologically active, such as an oligo- or polypeptide that, when cleaved from the moieties, binds a receptor, deactivates an enzyme, etc. Various oligomeric linkages that are biologically compatible and/or bioerodible are known in the art, and the selection of the linkage may influence the ultimate properties of the material, such as whether it is durable when implanted, whether it gradually deforms or shrinks after implantation, or whether it gradually degrades and is absorbed by the body. The linkage may be attached to the moieties by any suitable bond or functional group, including carbon-carbon bonds, esters, ethers, amides, amines, carbonates, carbamates, sulfonamides, etc.

In one exemplary embodiment, the crosslinking molecule comprises moieties that are biologically active drugs joined by a linkage that is biologically active and hydrolyzes under physiological conditions. After implantation, the linkages are gradually cleaved, releasing the active drugs and partially degrading the structure of the material. If the polymer supporting the cyclodextrin is also biodegradable, the material will gradually disintegrate, slowly releasing the biologically active drugs complexed within it. In such embodiments, additional pharmaceutical agents may, but need not be, included in the material to obtain a therapeutic effect.

Materials of the invention may further comprise one or more biologically active agents. Such agents may also form inclusion complexes with cyclodextrin, or may be merely dispersed through the material. Exemplary agents include nucleic

acids, viruses, polypeptides, polyplexes, pharmaceuticals, small organic molecules, antibodies, or any other therapeutic agents.

In certain embodiments, a subject composition comprises an RNAi construct, e.g., for using RNA interference (RNAi) to effect knockdown of a target gene.

5 RNAi constructs comprise double stranded RNA that can specifically block expression of a target gene, and are suitable for delivery using the subject compositions. RNAi provides a useful method of inhibiting gene expression in vitro or in vivo. RNAi constructs can comprise either long stretches of dsRNA identical or substantially identical to the target nucleic acid sequence or short stretches of

10 dsRNA identical to substantially identical to only a region of the target nucleic acid sequence.

Optionally, the RNAi constructs contain a nucleotide sequence that hybridizes under physiologic conditions of the cell to the nucleotide sequence of at least a portion of the mRNA transcript for the gene to be inhibited (i.e., the “target”

15 gene). The double-stranded RNA need only be sufficiently similar to natural RNA that it has the ability to mediate RNAi. Thus, the invention has the advantage of being able to tolerate sequence variations that might be expected due to genetic mutation, strain polymorphism or evolutionary divergence. The number of tolerated nucleotide mismatches between the target sequence and the RNAi construct

20 sequence is no more than 1 in 5 basepairs, or 1 in 10 basepairs, or 1 in 20 basepairs, or 1 in 50 basepairs. Mismatches in the center of the siRNA duplex are most critical and may essentially abolish cleavage of the target RNA. In contrast, nucleotides at the 3' end of the siRNA strand that is complementary to the target RNA do not significantly contribute to specificity of the target recognition. Sequence identity

25 may be optimized by sequence comparison and alignment algorithms known in the art (see Gribskov and Devereux, Sequence Analysis Primer, Stockton Press, 1991, and references cited therein) and calculating the percent difference between the nucleotide sequences by, for example, the Smith-Waterman algorithm as implemented in the BESTFIT software program using default parameters (e.g.,

30 University of Wisconsin Genetic Computing Group). Greater than 90% sequence identity, or even 100% sequence identity, between the inhibitory RNA and the

portion of the target gene is preferred. Alternatively, the duplex region of the RNA may be defined functionally as a nucleotide sequence that is capable of hybridizing with a portion of the target gene transcript (e.g., 400 mM NaCl, 40 mM PIPES pH 6.4, 1 mM EDTA, 50 °C or 70 °C hybridization for 12-16 hours; followed by
5 washing).

The double-stranded structure may be formed by a single self-complementary RNA strand or two complementary RNA strands. RNA duplex formation may be initiated either inside or outside the cell. The RNA may be introduced in an amount which allows delivery of at least one copy per cell. Higher doses (e.g., at least 5, 10,
10 100, 500 or 1000 copies per cell) of double-stranded material may yield more effective inhibition, while lower doses may also be useful for specific applications. Inhibition is sequence-specific in that nucleotide sequences corresponding to the duplex region of the RNA are targeted for genetic inhibition.

The subject RNAi constructs can be "small interfering RNAs" or "siRNAs."
15 These nucleic acids are around 19-30 nucleotides in length, and even more preferably 21-23 nucleotides in length. The siRNAs are understood to recruit nuclease complexes and guide the complexes to the target mRNA by pairing to the specific sequences. As a result, the target mRNA is degraded by the nucleases in the protein complex. In a particular embodiment, the 21-23 nucleotides siRNA
20 molecules comprise a 3' hydroxyl group. In certain embodiments, the siRNA constructs can be generated by processing of longer double-stranded RNAs, for example, in the presence of the enzyme dicer. In one embodiment, the *Drosophila in vitro* system is used. In this embodiment, dsRNA is combined with a soluble extract derived from *Drosophila* embryo, thereby producing a combination. The
25 combination is maintained under conditions in which the dsRNA is processed to RNA molecules of about 21 to about 23 nucleotides. The siRNA molecules can be purified using a number of techniques known to those of skill in the art. For example, gel electrophoresis can be used to purify siRNAs. Alternatively, non-denaturing methods, such as non-denaturing column chromatography, can be used to
30 purify the siRNA. In addition, chromatography (e.g., size exclusion

chromatography), glycerol gradient centrifugation, affinity purification with antibody can be used to purify siRNAs.

Production of RNAi constructs can be carried out by chemical synthetic methods or by recombinant nucleic acid techniques. Endogenous RNA polymerase of the treated cell may mediate transcription *in vivo*, or cloned RNA polymerase can be used for transcription *in vitro*. The RNAi constructs may include modifications to either the phosphate-sugar backbone or the nucleoside, e.g., to reduce susceptibility to cellular nucleases, improve bioavailability, improve formulation characteristics, and/or change other pharmacokinetic properties. For example, the phosphodiester linkages of natural RNA may be modified to include at least one of an nitrogen or sulfur heteroatom. Modifications in RNA structure may be tailored to allow specific genetic inhibition while avoiding a general response to dsRNA. Likewise, bases may be modified to block the activity of adenosine deaminase. The RNAi construct may be produced enzymatically or by partial/total organic synthesis, any modified ribonucleotide can be introduced by *in vitro* enzymatic or organic synthesis. Methods of chemically modifying RNA molecules can be adapted for modifying RNAi constructs (see, e.g., Heidenreich et al. (1997) Nucleic Acids Res. 25:776-780; Wilson et al. (1994) J Mol Recog 7:89-98; Chen et al. (1995) Nucleic Acids Res 23:2661-2668; Hirschbein et al. (1997) Antisense Nucleic Acid Drug Dev 7:55-61). Merely to illustrate, the backbone of an RNAi construct can be modified with phosphorothioates, phosphoramidate, phosphodithioates, chimeric methylphosphonate-phosphodiester, peptide nucleic acids, 5-propynyl-pyrimidine containing oligomers or sugar modifications (e.g., 2'-substituted ribonucleosides, α -configuration).

In some cases, at least one strand of the siRNA molecules has a 3' overhang from about 1 to about 6 nucleotides in length, though may be from 2 to 4 nucleotides in length. More preferably, the 3' overhangs are 1-3 nucleotides in length. In certain embodiments, one strand having a 3' overhang and the other strand being blunt-ended or also having an overhang. The length of the overhangs may be the same or different for each strand. In order to further enhance the stability of the siRNA, the 3' overhangs can be stabilized against degradation. In one embodiment, the RNA is

stabilized by including purine nucleotides, such as adenosine or guanosine nucleotides. Alternatively, substitution of pyrimidine nucleotides by modified analogues, e.g., substitution of uridine nucleotide 3' overhangs by 2'-deoxythyridine is tolerated and does not affect the efficiency of RNAi. The absence of a 2' hydroxyl
5 significantly enhances the nuclease resistance of the overhang in tissue culture medium and may be beneficial *in vivo*.

The RNAi construct can also be in the form of a long double-stranded RNA. In certain embodiments, the RNAi construct is at least 25, 50, 100, 200, 300 or 400 bases. In certain embodiments, the RNAi construct is 400-800 bases in length. The
10 double-stranded RNAs are digested intracellularly, e.g., to produce siRNA sequences in the cell. However, use of long double-stranded RNAs *in vivo* is not always practical, presumably because of deleterious effects which may be caused by the sequence-independent dsRNA response. In such embodiments, the use of local delivery systems and/or agents which reduce the effects of interferon or PKR are
15 preferred.

Alternatively, the RNAi construct is in the form of a hairpin structure (named as hairpin RNA). The hairpin RNAs can be synthesized exogenously or can be formed by transcribing from RNA polymerase III promoters *in vivo*. Examples of making and using such hairpin RNAs for gene silencing in mammalian cells are
20 described in, for example, Paddison et al., Genes Dev, 2002, 16:948-58; McCaffrey et al., Nature, 2002, 418:38-9; McManus et al., RNA, 2002, 8:842-50; Yu et al., Proc Natl Acad Sci U S A, 2002, 99:6047-52). Preferably, such hairpin RNAs are engineered in cells or in an animal to ensure continuous and stable suppression of a desired gene. It is known in the art that siRNAs can be produced by processing a
25 hairpin RNA in the cell.

PCT application WO 01/77350 describes an exemplary vector for bi-directional transcription of a transgene to yield both sense and antisense RNA transcripts of the same transgene in a eukaryotic cell. Accordingly, in certain embodiments, a subject composition includes, for ultimate delivery, a recombinant
30 vector having the following unique characteristics: it comprises a viral replicon having two overlapping transcription units arranged in an opposing orientation and

flanking a transgene for an RNAi construct of interest, wherein the two overlapping transcription units yield both sense and antisense RNA transcripts from the same transgene fragment in a host cell.

V. Business Methods

5 Other aspects of the invention provides for certain methods of doing business. In particular, practicing the methods of the invention may enable novel therapeutic compositions and improved formulations thereof. This technical step, when combined with one or more additional steps, provides for novel approaches to conducting a pharmaceutical, or preferably a life-science business. For example, a
10 therapeutic composition prepared by the method of the invention may be tested for efficacy as therapeutics in a variety of disease models, the potential therapeutic compositions then tested for toxicity and other safety-profiling before formulating, packaging and subsequently marketing the resulting formulation for the treatment of disease. Alternatively, the rights to develop and market such formulations or to
15 conduct such steps may be licensed to a third party for consideration.

Accordingly, in certain embodiments, the present invention provides a method for conducting a pharmaceutical business, comprising:

- a. manufacturing a formulation or kit including a pharmaceutical composition of any of the compositions disclosed herein; and
- 20 b. marketing to healthcare providers the benefits of using the formulation or kit in the treatment of a disease or disorder.

In other embodiments, the present invention discloses a method for conducting a pharmaceutical business, comprising:

- a. providing a distribution network for selling a pharmaceutical
25 composition of any of the compositions disclosed herein; and
- b. providing instruction material to patients or physicians for using the preparation in the treatment of a disease or disorder.

In certain embodiments, the present invention provides a method for conducting a pharmaceutical business, comprising:

- a. determining an appropriate formulation and dosage of a pharmaceutical composition of any of the compositions disclosed herein;
- 5 b. conducting therapeutic profiling of formulations identified in step (a), for efficacy and toxicity in animals; and
- c. providing a distribution network for selling a preparation or preparations identified in step (b) as having an acceptable therapeutic profile.

10 An additional step of the embodiment comprises providing a sales group for marketing the preparation to healthcare providers.

In still other embodiments, the present invention provides a method for conducting a pharmaceutical business, comprising:

- a. determining an appropriate formulation and dosage of a pharmaceutical composition of any of the compositions disclosed herein; and
- 15 b. licensing, to a third party, the rights for further development and sale of the formulation.

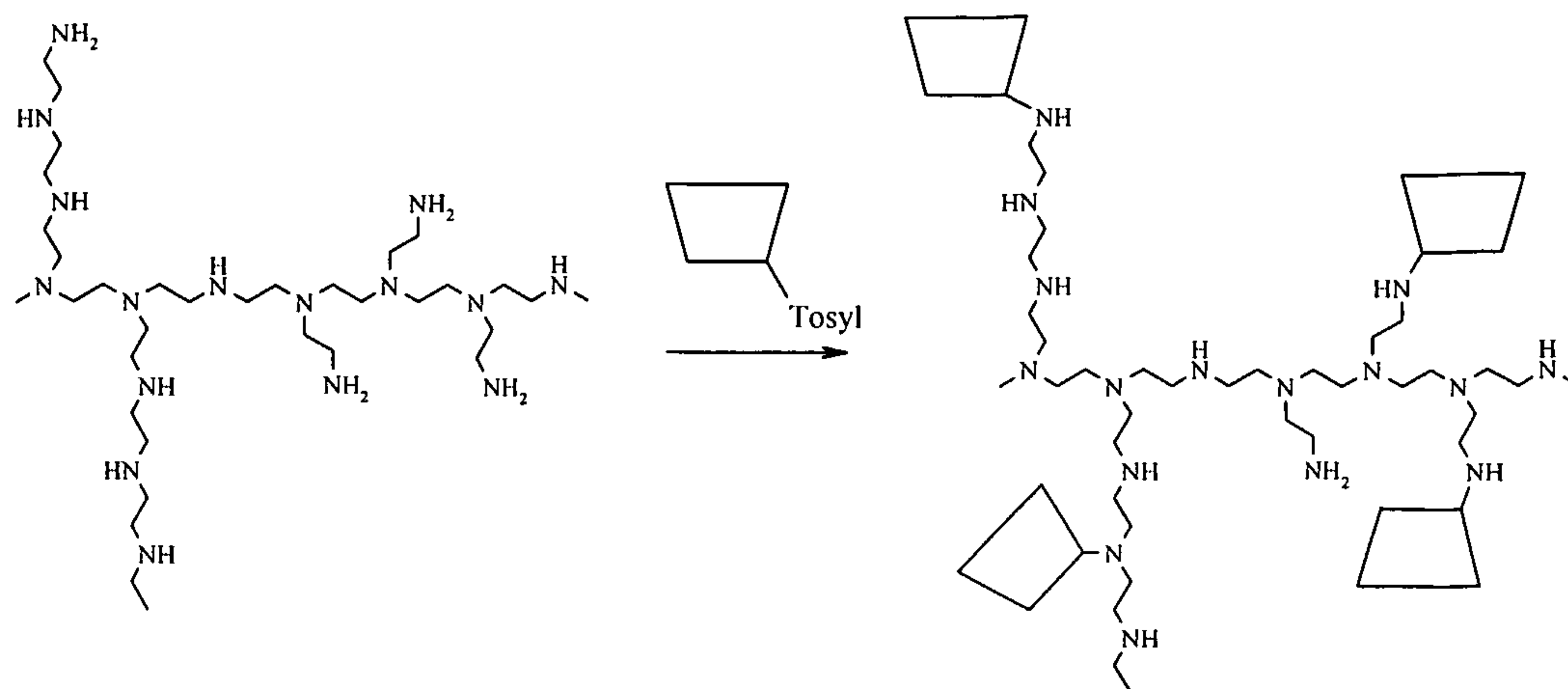
Exemplification

20 The invention now being generally described, it will be more readily understood by reference to the following examples, which are included merely for purposes of illustration of certain aspects and embodiments of the present invention, and are not intended to limit the invention.

Example 1

Synthesis of Polyethylenimine (PEI)-Cyclodextrin Conjugates

25 (Suh et al. 1992, J. Am. Chem. Soc. 114 7916-7917)

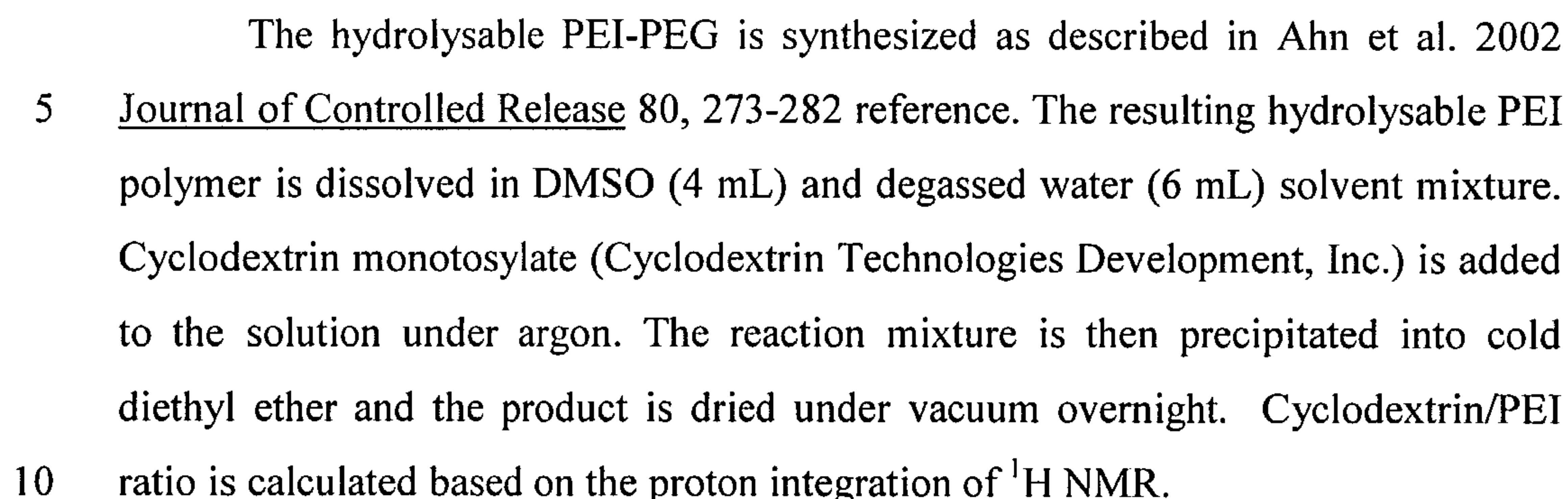


Branched PEI (60 mg, Aldrich Mw 25,000) was dissolved in DMSO (4 mL)
 5 and degassed water (6 mL) solvent mixture. Cyclodextrin monotosylate (928 mg,
 Cyclodextrin Technologies Development, Inc.) was added to the solution under
 argon. The cloudy solution turned clear after the mixture was stirred at 70 °C for
 about 1 hour. The solution turned slightly yellow after 48 hours at this temperature
 under argon. The solution was transferred to a Spectra/Por MWCO 25,000
 10 membrane and dialyzed against water for 6 days. Water was then removed by
 lyophilization. A white powder was obtained (134 mg) after the solution was
 lyophilized. Cyclodextrin/PEI ratio was calculated based on the proton integration
 of ^1H NMR.

15 Example 2

Synthesis of hydrolysable Polyethylenimine (PEI)-Cyclodextrin Conjugates

Ahn et al. 2002 Journal of Controlled Release 80, 273-282

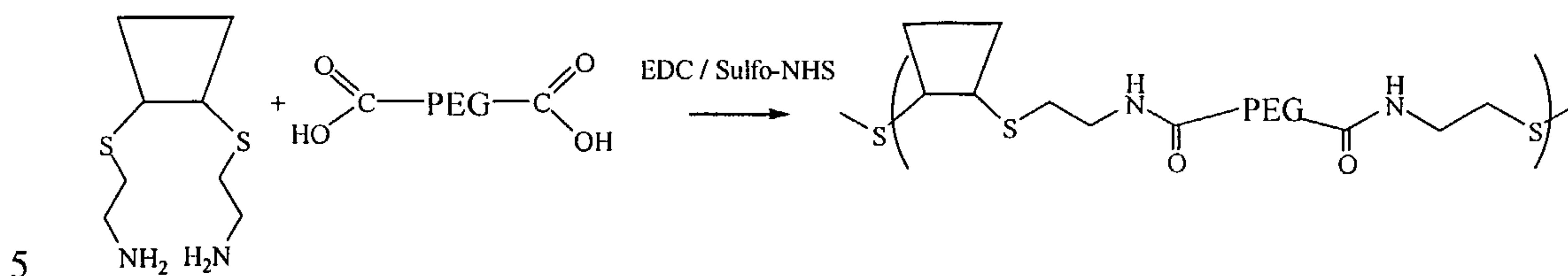


Synthesis of linear Cyclodextrin-based polyethylene glycol polymers (CD-PEG)

- 44 -

was carried using commercially available difunctionalized polyethylene glycol. Three methods were investigated.

Method I: Using diacid-polyethylene glycol



Synthesis:

Diacid-PEGs with various molecular weights ($M_w = 250, 600, 3000, 6000$) were purchased from Fluka, Milwaukee, WI. In a typical experiment, PEG₆₀₀-(COOH)₂ (0.096 g, 0.16 mmol) was dissolved in 1 mL of a 25 mM MES buffer (2-(N-morpholino)ethanesulfonic acid) at pH 6.5. Dicysteamine- β -cyclodextrin (0.2 g, 0.16 mmol) dissolved in 2 mL of a 25 mM MES buffer (pH 6.5) was added. Then, 1-(3-dimethylaminopropyl)-3-ethylcarbodiimide hydrochloride (EDC) (0.612 g, 3.2 mmol, Aldrich, Milwaukee, WI) and N-Hydroxysulfosuccinimide (Sulfo-NHS) (0.026 g, 0.12 mmol, Pierce, Rockford, IL) were added. The resulting solution was allowed to stir overnight at room temperature. The polymer solution was then transferred to a Spectra/Por 7 MWCO 10,000 membrane (Spectrum, Houston, TX) and dialyzed against water for 24 h. The solution was then freeze-dried to dryness. This afforded 272 mg of white solid (Yield: 93%).

20 Characterization: Light Scattering and Molecular Weight Determination

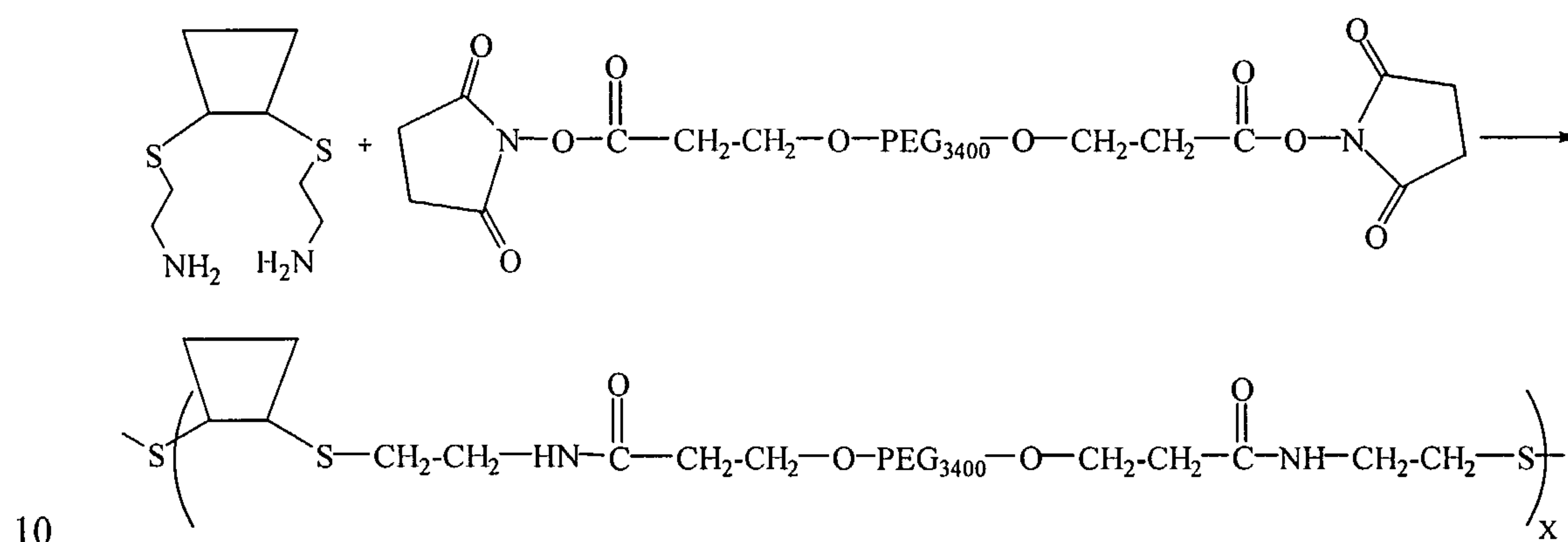
The specific refractive index increment, dn/dc , was measured in Phosphate Buffered Saline 1x (PBS) (Cellgro, Mediatech, Inc, Herndon, VA) using a Bausch & Lomb ABBE-3L refractive index. Polymer samples were then analyzed on a Hitachi D6000 HPLC system equipped with a ERC-7512 RI detector, a Precision Detectors PD2020/DLS static light scattering detector and an PL aquagel-OH 30 (Polymer Laboratories, Amherst, MA) column using Phosphate Buffered Saline 1x as eluant at a 0.7 mL/min flow rate. The dn/dc , the weight average molecular weight M_w , and

the polydispersity index M_w/M_n determined for each polymer are reported in the following table.

Table 1: Static Light Scattering and Molecular Weight Determination of CD-PEG
5 polymers.

Polymer	dn/dc	Mw (Da)	Polydispersity
CD-PEG ₆₀₀₀	0.1267	21,560	1.69
CD-PEG ₃₀₀₀	0.1296	10,490	1.35
CD-PEG ₆₀₀	0.1361	28,450	1.77
CD-PEG ₂₅₀	0.1359	21,150	1.06

Method II: Using disuccinimidyl propionate polyethylene glycol



Synthesis:

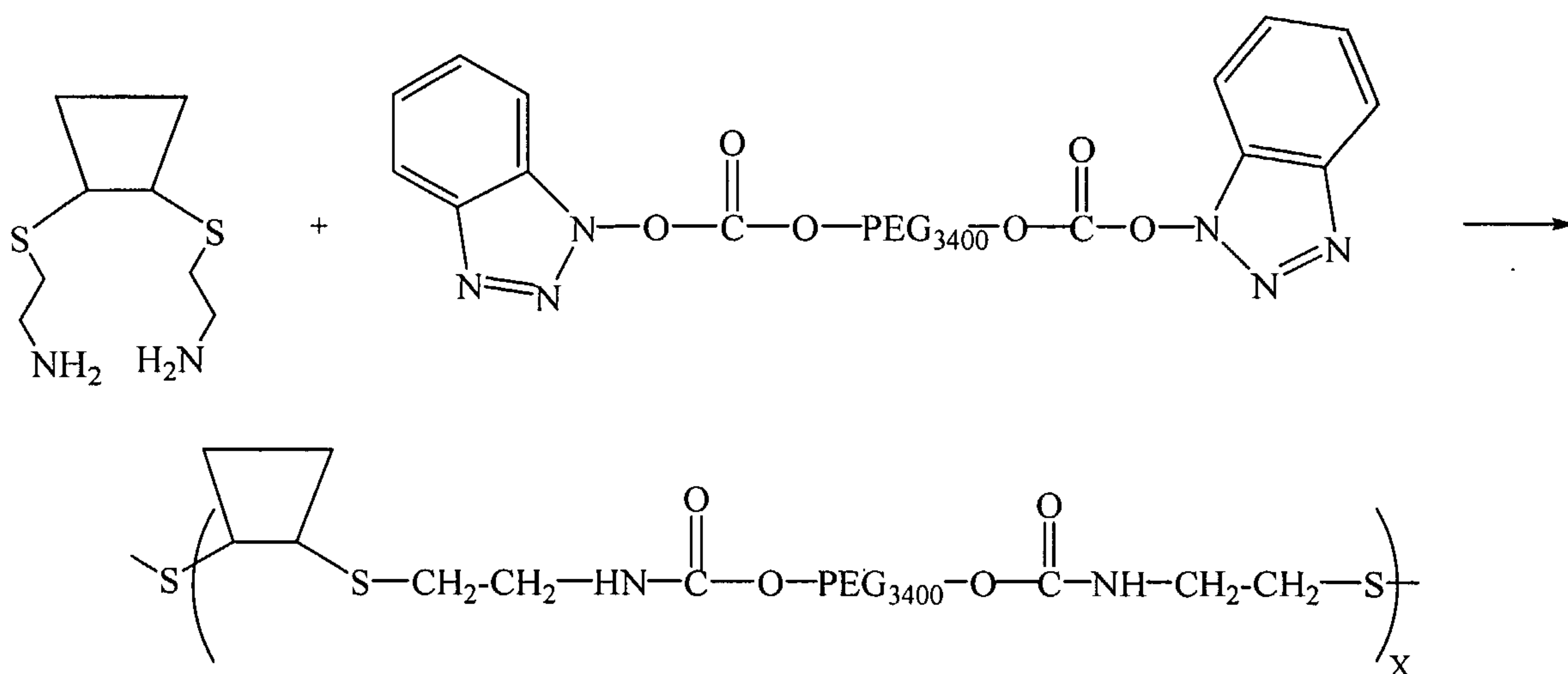
Disuccinimidyl propionate polyethylene glycol (PEG₃₄₀₀-(SPA)₂) (1.0854 g, 0.32
15 mmol, Shearwater Polymers, Inc, Huntsville, AL) in solution in 5 mL of DMSO was
added to a solution of dicysteamine- β -cyclodextrin (0.4 g, 0.32 mmol) dissolved in 2
mL of DMSO. A viscous solution was immediately formed. The reaction mixture

was then allowed to stir overnight at room temperature under argon. Diethylether was added to precipitate the polymer and then poured out with a pipet. The residual ether was evaporated and the polymer was redissolved in water. The resulting solution was then transferred to a 10,000 MWCO Spectra/Por membrane and dialyzed against water for 24 h. The solution was then freeze-dried to dryness. This
 5 afforded 1.329 g of white solid (Yield: 95%).

Characterization: Light Scattering and Molecular Weight Determination

This polymer was characterized using the same technique presented above. The dn/dc was calculated to be 0.1316 and the weight average molecular weight M_w was
 10 determined to be 184,000 Da with a polydispersity index M_w/M_n of 2.18.

Method III: Using di-benzotriazole carbonate polyethylene glycol



15 Synthesis:

Di-benzotriazole carbonate polyethylene glycol (PEG₃₄₀₀-(BTC)₂) (1 g, 0.32 mmol, Shearwater Polymers, Inc, Huntsville, AL) in solution in 5 mL of DMSO was added to a solution of dicysteamine-β-cyclodextrin (0.4 g, 0.32 mmol) dissolved in 2 mL of DMSO. A viscous solution was immediately formed. The reaction mixture was then
 20 allowed to stir overnight at room temperature under argon. Diethyl ether was added

to precipitate the polymer and then poured out with a pipette. The residual ether was evaporated and the polymer was redissolved in water. The resulting solution was then transferred to a 10,000 MWCO Spectra/Por membrane and dialyzed against water for 24 h. The solution was then freeze-dried to dryness. This afforded 1.3 g of
 5 white solid (Yield: 95%).

Example 4

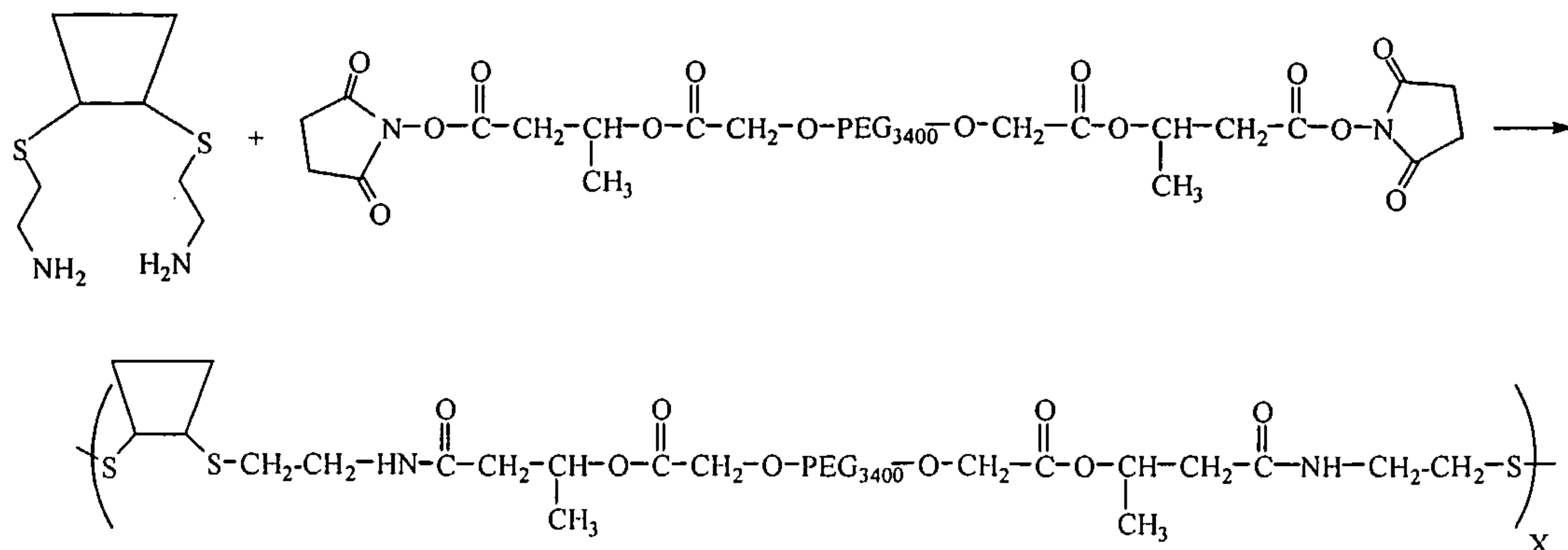
Molecular weight control of CD-PEG polymers:

Dicysteamine- β -cyclodextrin•2 HCl (0.577 g, 0.46 mmol) was dried under vacuum at 100 °C for 16 h. Disuccinimidyl propionate polyethylene glycol (PEG₃₄₀₀-
 10 (SPA)₂) (1.565 g, 0.46 mmol, Shearwater Polymers, Inc, Huntsville, AL) was then added. To the mixture was added dry DMSO (8 mL). After 10 min stirring, DIEA (176 μ L, 1.01 mmol) was added under argon. A portion of polymerization solution (1 mL) was removed at selected times (15 min, 30 min, 60 min, 1 h, 2 h and 5 h). These samples were then transferred to a 10,000 MWCO Spectra/Por membrane and
 15 dialyzed against water for 24 h. The solutions were then freeze-dried to dryness. MWs of the resulting solids were determined as described above.

As shown in Figure 3, the polymer Mw increased to around 80 kDa over a 5 h time course. The polymer Mw can be controlled between 50 to 80 kDa.
 5

20 *Synthesis of hydrolysable linear cyclodextrin-based polyethylene glycol polymers (CD-PEG)*

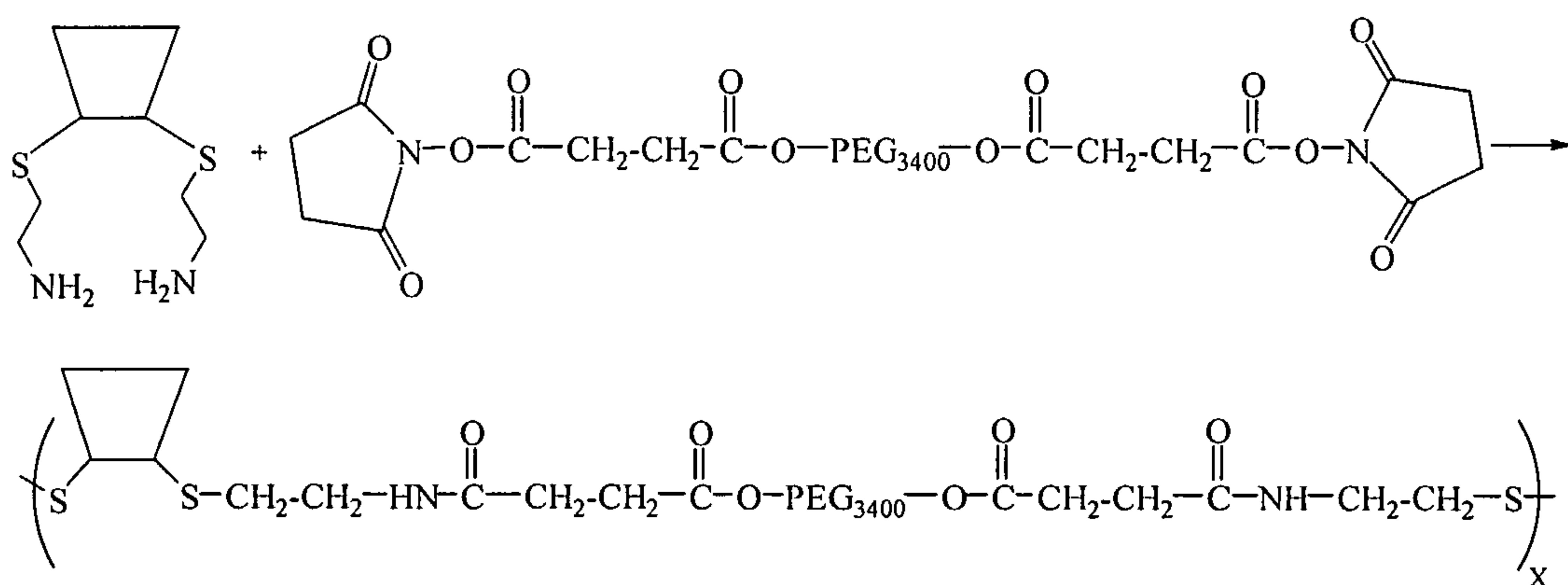
Method I: Using NHS-HBA-CM-PEG₃₄₀₀-CM-HBA-NHS



NHS-HBA-CM-PEG₃₄₀₀-CM-HBA-NHS (0.2 g, 0.06 mmol, Shearwater Polymers, Inc, Huntsville, AL) in solution in 1.5 mL of DMSO is added to a solution of
 5 dicysteamine-β-cyclodextrin (0.074 g, 0.06 mmol) dissolved in 2 mL of DMSO. The reaction mixture is then allowed to stir overnight at room temperature under argon. The resulting polymer is precipitated with diethylether, filtrated and dried under vacuum.

10

Method II: Using PEG succinimidyl succinate (PEG-(SS)₂)



Synthesis:

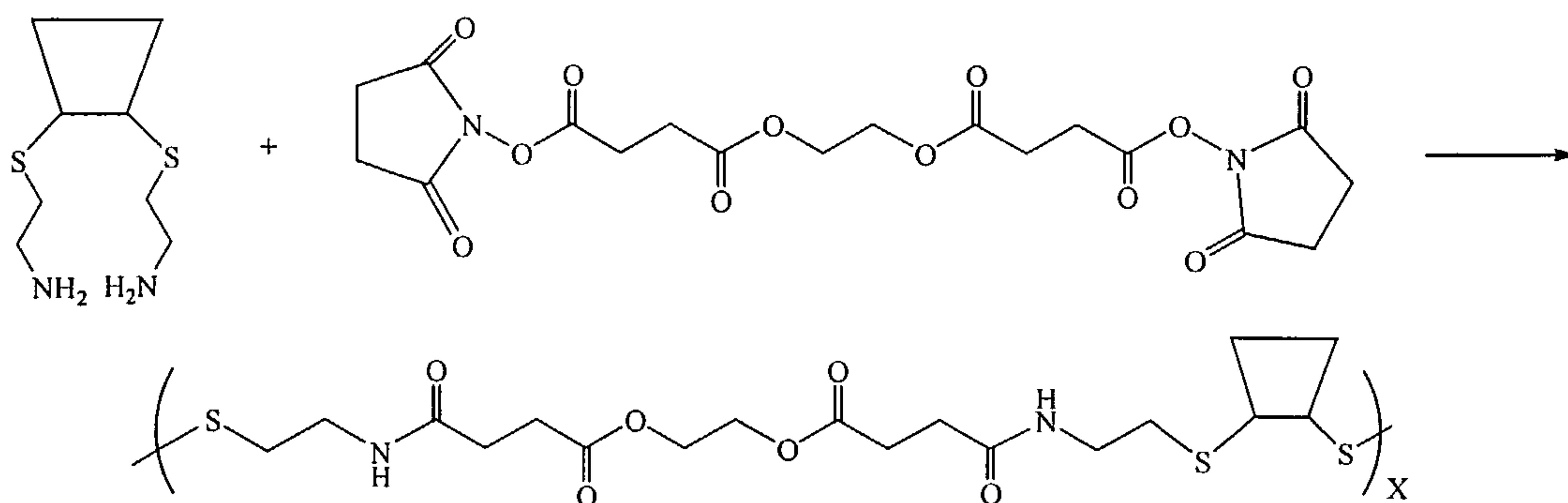
15 Disuccinimidyl succinate polyethylene glycol (PEG₃₄₀₀-(SS)₂) (SunBio, Inc., 980-5 Kwan-yang Dong, Anyang City, S. Korea) (0.3 mmol) in solution in 5 mL of DMSO

is added to a solution of dicysteamine- β -cyclodextrin (0.3 mmol) dissolved in 2 mL of DMSO. The reaction mixture is then allowed to stir overnight at room temperature under argon. The resulting polymer is precipitated with diethylether, filtrated and dried under vacuum.

5

Example 6

Synthesis of hydrolysable linear cyclodextrin-based polymer



10

Synthesis:

Ethylene glycol bis[succinimidylsuccinate] (EGS) (0.2 mmol, Pierce, Rockford, IL) in solution in 2 mL of DMSO is added to a solution of dicysteamine- β -cyclodextrin (0.2 mmol) dried overnight at 100 °C under vacuum and dissolved in 1.5 mL of DMSO. The reaction mixture is then allowed to stir overnight at room temperature under argon. The resulting mixture is precipitated with Acetone, filtrated and dried under vacuum.

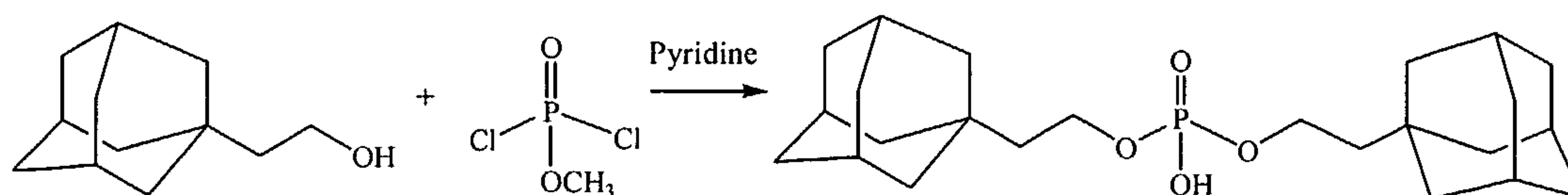
15

Example 7

Synthesis of diadamantane crosslinker: Bis-(2(1-adamantyl)ethyl)phosphate

(Zhang et al. 1997, J. Am. Chem. Soc. 119(7):1676-1681)

20



Synthesis:

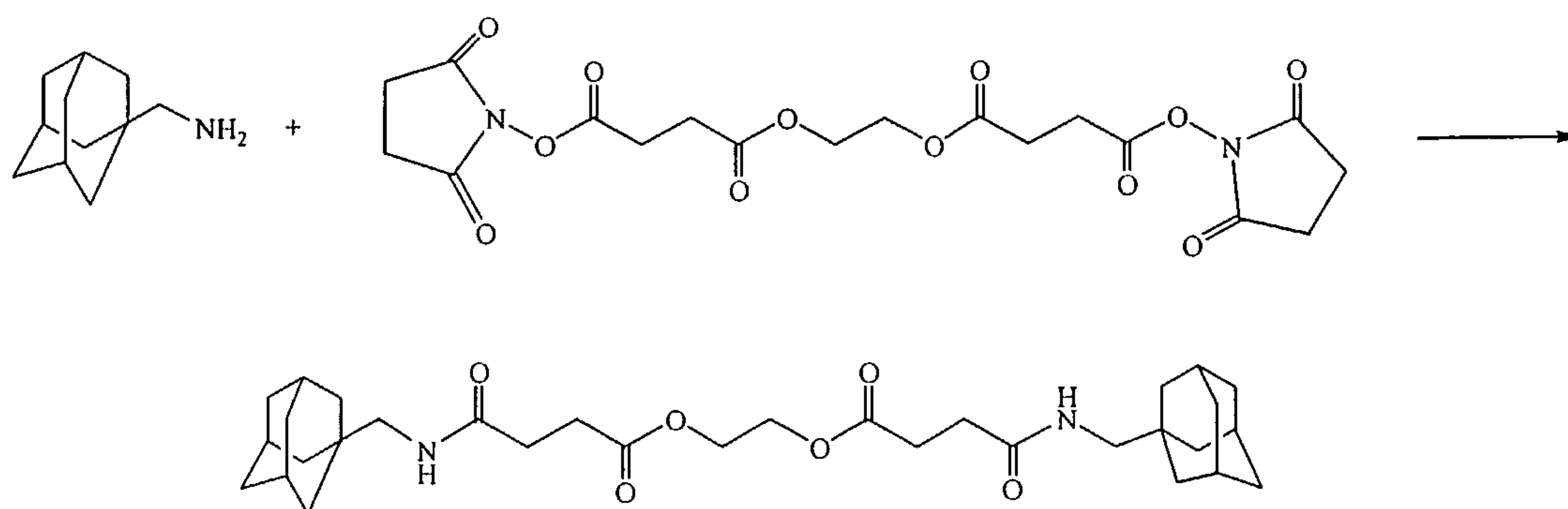
- 5 Anydrous pyridine (10 mL, Aldrich, Milwaukee, WI) was cooled in an ice bath and methyl dichlorophosphate (1.488 g, 10 mmol, Aldrich, Milwaukee, WI) was added dropwise. The mixture was kept cold for a further 15 min. During this period a precipitate of N-methylpyridinium dichlorophosphate formed. 1-Adamantane ethanol (4.758 g, 26.4 mmol, Aldrich, Milwaukee, WI) was added, and the sealed
- 10 mixture was stirred overnight at room temperature. It was then poured into 10% NaHCO₃ (50 mL) and the pyridine was evaporated under vacuum. The slightly yellow solid was dissolved in 1 L of water and extracted with ether (three 150 mL portions). The aqueous phase was acidified with 2 N HCl to pH 1, and then extracted with three 150 mL portions of CHCl₃:*n*-BuOH (7:3). The combined organic layer
- 15 (ether and CHCl₃:*n*-BuOH) was washed with water and a slightly yellow precipitate was formed in the mixed solvents, at which point the solvents were evaporated under vacuum. A slightly yellow solid was formed and was recrystallized from acetone/hexane. The solid was dried under vacuum, yield 60 %.

Characterization:

- 20 The product was characterized by ¹H NMR and ¹³C NMR. ¹H NMR (CDCl₃): δ 1.45-1.75 (m, 28H, -CH₂-, adamantyl), 1.95 (m, 6H, C-H, adamantyl), 4.07 (q, 4H, -CH₂-) and 8.60 (br, 1H, POOH). ¹³C NMR (CDCl₃, 500MHz): δ 28.59, 31.77, 37.02, 42.52, 43.96, 44.02, 64.21, 64.26. The product was also characterized by Mass Spectroscopy: Electrospray Ionization: 421 [M-H]⁻.

25 **Example 8**

Synthesis of hydrolysable adamantane crosslinker:

Synthesis:

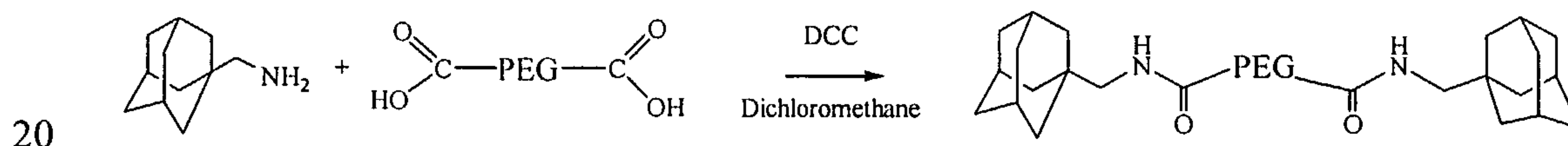
1-Adamantanemethylamine (0.152 g, 0.92 mmol, Aldrich, Milwaukee, WI) was added to Ethylene glycol bis[succinimidylsuccinate] (EGS) (0.2 g, 0.43 mmol, Pierce, Rockford, IL) in solution in 10 mL of anhydrous dichloromethane. The resulting solution was stirred for 5 h at room temperature. It was then acidified with 0.1 N HCl and extracted with dichloromethane. The organic phase was dried with MgSO₄ and then concentrated to dryness under vacuum. This afforded 0.22 g of solid (yield 90%).

Characterization:

The product was characterized by Mass Spectroscopy: Electrospray Ionization: 557 [M+H]⁺, 579 [M+Na]⁺, 1135 [2M+Na]⁺.

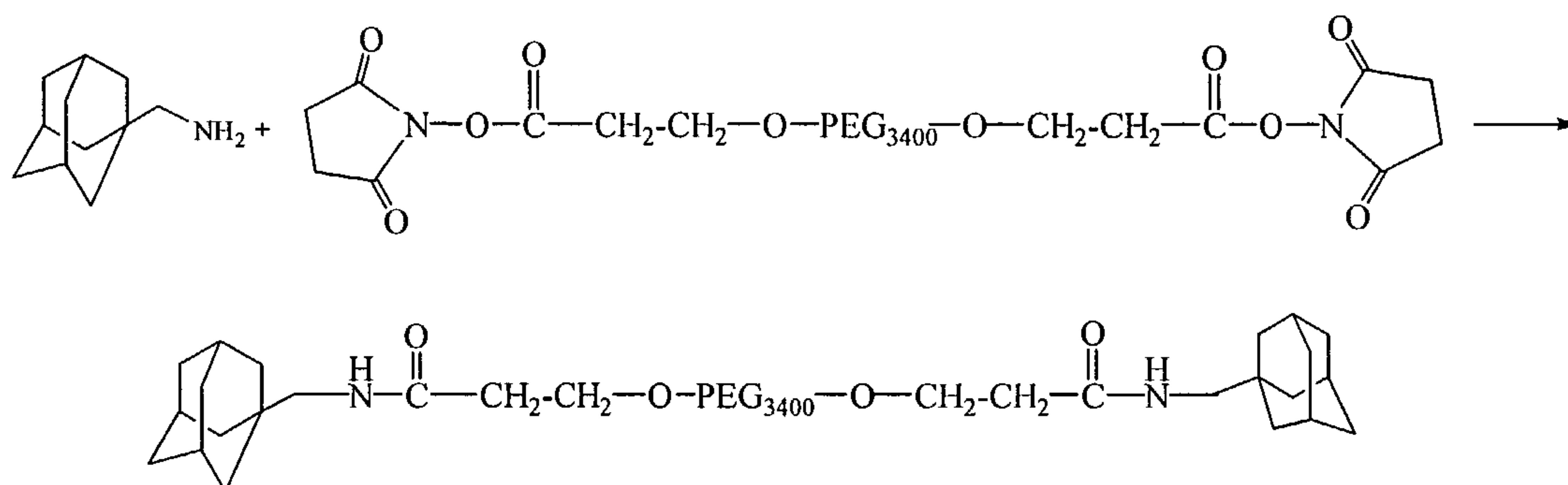
15 **Example 9***Synthesis of diadamantane polyethylene glycol crosslinker:*

Various methods were investigated:

Method I: Using diacid-polyethylene glycol

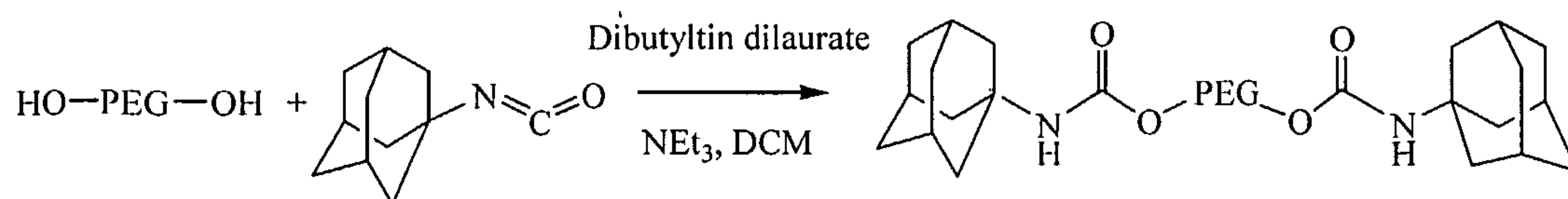
1-Adamantanemethylamine (0.64 mmol, Aldrich, Milwaukee, WI) is added to PEG-diacid (0.32 mmol, Fluka, Milwaukee, WI) dissolved in dichloromethane. 1,3-Dicyclohexylcarbodiimide (DCC) (3.2 mmol, Aldrich, Milwaukee, WI) is added and the resulting solution is stirred overnight at room temperature. The precipitate (dicyclohexylisourea, DCU) is filtered off and the filtrate is washed with 18% HCl. The organic phase is dried with MgSO_4 and then concentrated to dryness under vacuum. The resulting solid is redissolved in water in order to precipitate the remaining DCC. DCC is filtered off and the filtrate is freeze-dried.

10 Method II: Using disuccinimidyl propionate polyethylene glycol



1-Adamantanemethylamine (0.1 g, 0.60 mmol, Aldrich, Milwaukee, WI) was added to Disuccinimidyl propionate polyethylene glycol ($\text{PEG}_{3400}\text{-(SPA)}_2$) (1.02 g, 0.30 mmol, Shearwater Polymers, Inc, Huntsville, AL) dissolved in 10 mL of dichloromethane. The resulting solution was stirred at room temperature overnight. The solvent was evaporated under vacuum and the residue was dissolved in water and centrifuged to remove excess 1-adamantanemethylamine. The supernatant was then transferred to a 1,000 MWCO Spectra/Por membrane and dialyzed against water for 24h. The solution was then freeze-dried to dryness. This afforded 0.88 g of solid (yield 84%).

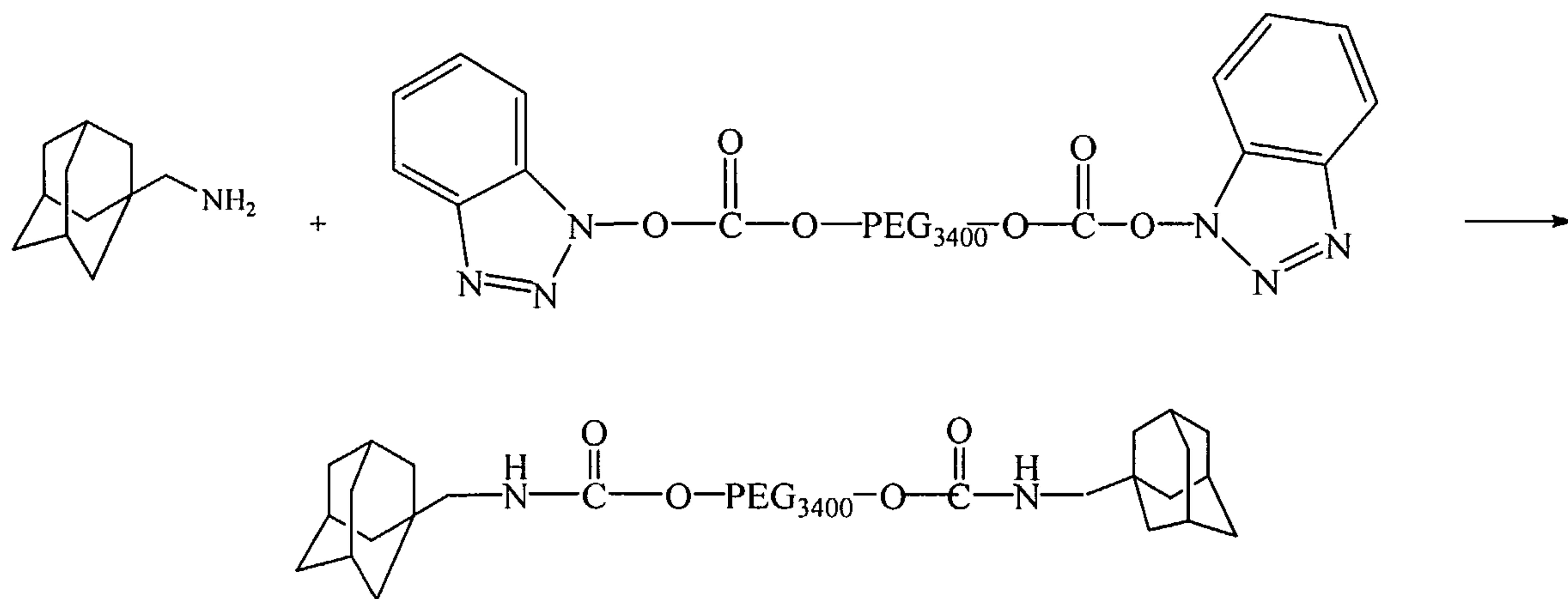
Method III: Using polyethylene glycol (Sandier et al. 2000, Langmuir 16:1634-1642)



- 5 Polyethylene glycol ($M_w = 1000$) (1g, 1mmol, Aldrich, Milwaukee, WI) was dried by heating under vacuum at 70 °C overnight. 1-Adamantyl isocyanate (0.39 g, 2.2 mmol, Aldrich, Milwaukee, WI) was added to the dried polyethylene glycol after its dissolution in anhydrous dichloromethane (25 mL). Two catalysts, dibutyltin dilaurate (63.2 mg, 0.1 mmol, Aldrich, Milwaukee, WI) and triethylamine (10.1 mg, 0.1 mmol, Aldrich, Milwaukee, WI) were then added. The reaction mixture was heated under reflux for 7 h. After removal of the solvent, the reaction product was dissolved in distilled water. The aqueous solution was purified by addition of activated carbon and successive filtrations, and then freeze-dried. The resulting polymer was recovered with a 70% yield and was characterized by ^1H NMR.

15

Method IV: Using di-benzotriazole carbonate polyethylene glycol



- 20 1-Adamantanemethylamine (0.1 g, 0.60 mmol, Aldrich, Milwaukee, WI) is added to Dibenzotriazole carbonate polyethylene glycol ($\text{PEG}_{3400}\text{-(BTC)}_2$) (1.02 g, 0.30 mmol, Shearwater Polymers, Inc, Huntsville, AL) dissolved in 10 mL of

dichloromethane. The resulting solution was stirred at room temperature overnight. The solvent was evaporated under vacuum and the residue was dissolved in water and centrifuged to remove excess 1-adamantanemethylamine. The supernatant was then transferred to a 1,000 MWCO Spectra/Por membrane and dialyzed against
 5 water for 24 h. The solution was then freeze-dried to dryness. This afforded 0.88 g of solid (yield 84%).

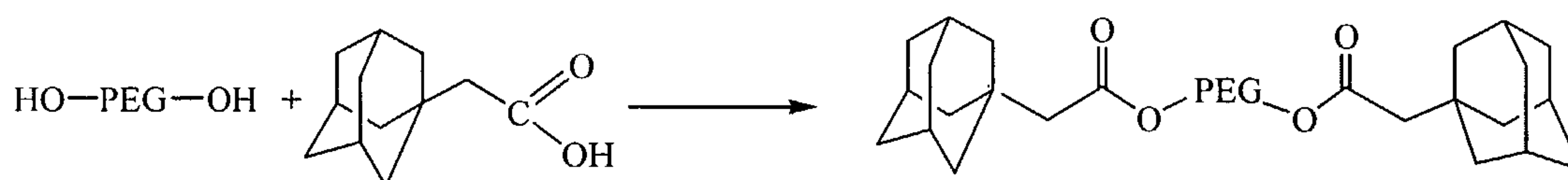
Example 10

Synthesis of hydrolysable diadamantane polyethylene glycol crosslinker:

Various methods were investigated:

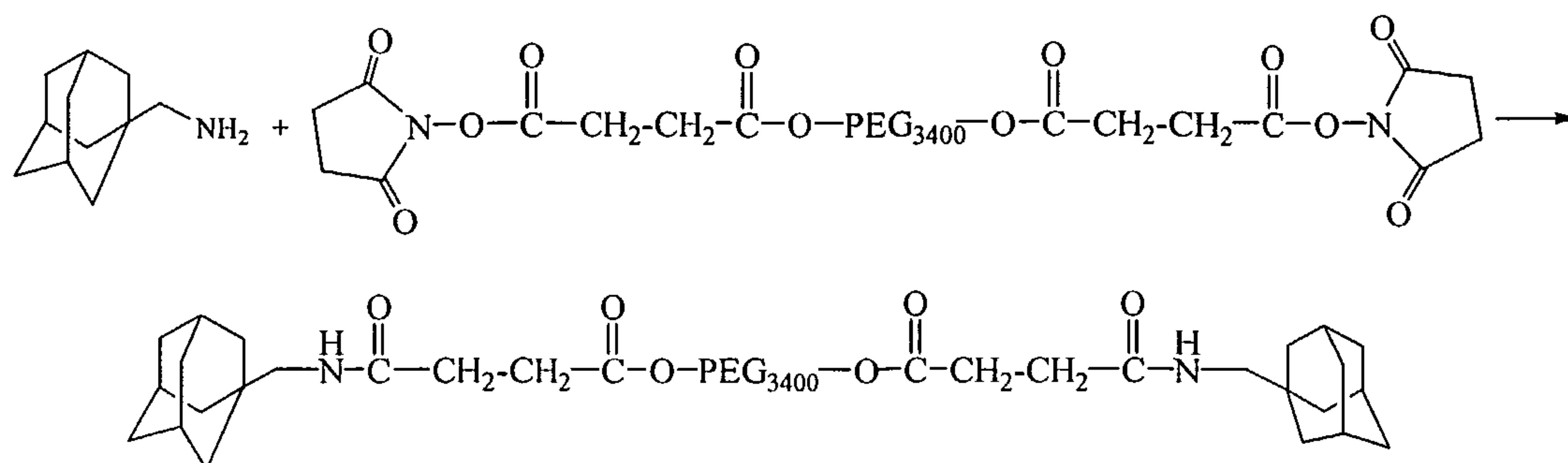
10

Method I: Using polyethylene glycol



Polyethylene glycol (Mw = 1000) (1 mmol, Aldrich, Milwaukee, WI) is dried by
 15 heating under vacuum at 70 °C overnight. 1-Adamantaneacetic acid (2.2 mmol, Aldrich, Milwaukee, WI) is added to the dried polyethylene glycol after its dissolution in anhydrous toluene (15 mL). *p*-Toluenesulfonic acid (Aldrich, Milwaukee, WI) is then added in a catalytic amount. The resulting mixture is azeotropically refluxed for 16 h using Dean-Stark apparatus. After completion of the
 20 reaction, the solvent is removed under vacuum and the resulting polymer is precipitated with ether.

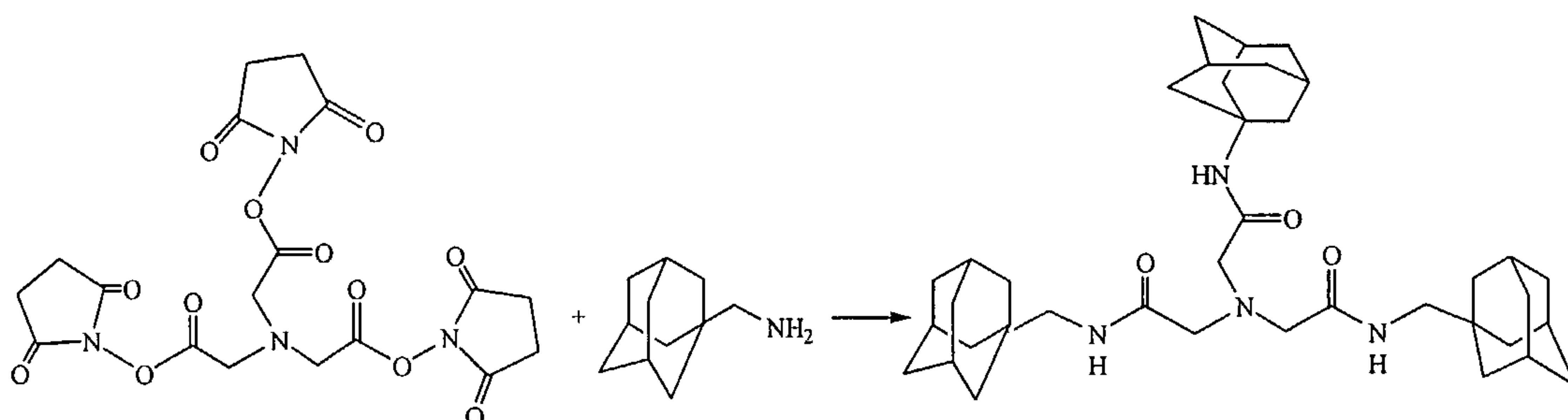
Method II: Using disuccinimidyl succinate polyethylene glycol



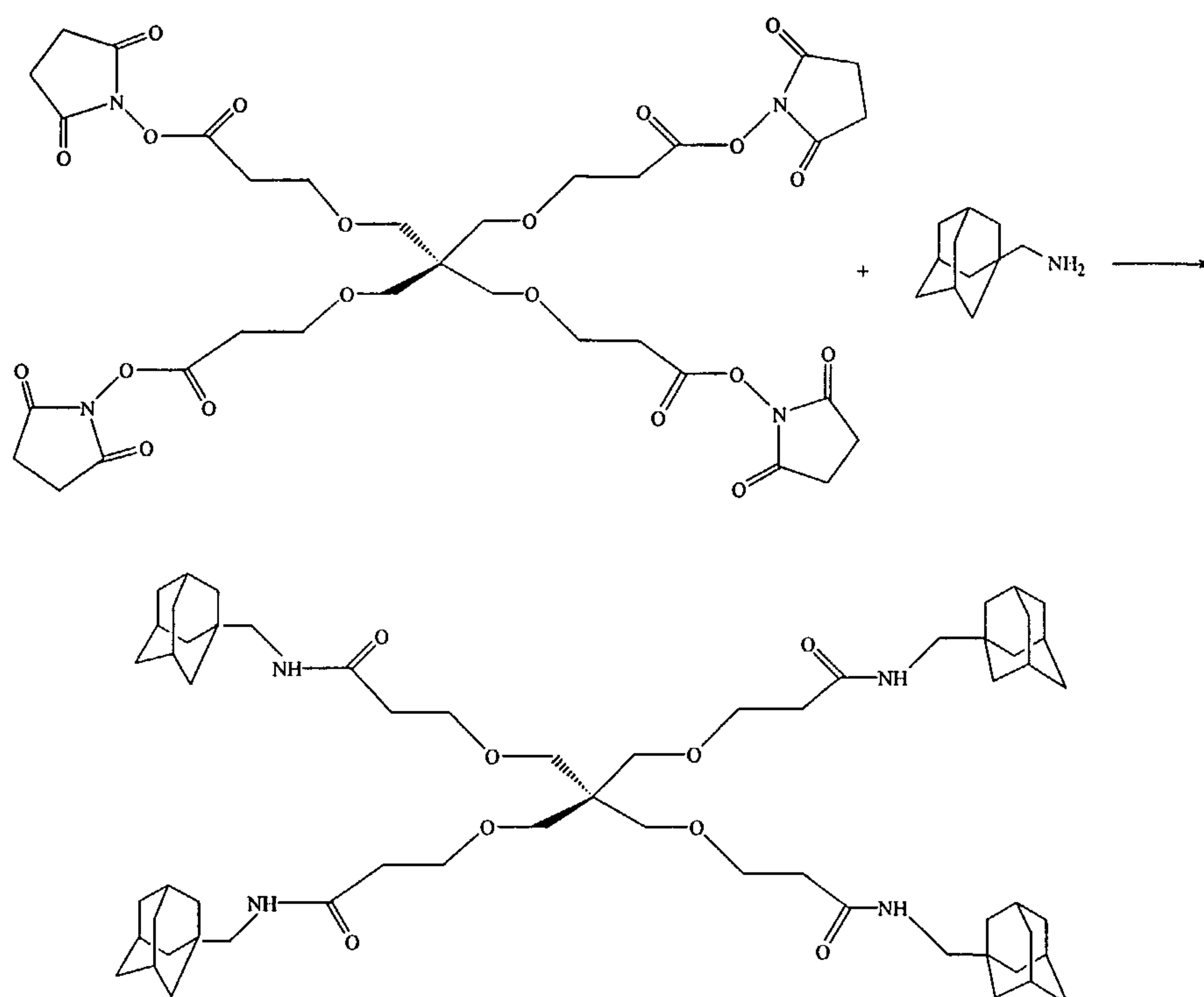
1-Adamantanemethylamine (0.1 g, 0.60 mmol, Aldrich, Milwaukee, WI) was added to disuccinimidyl succinate polyethylene glycol (PEG₃₄₀₀-(SS)₂) (SunBio, Inc., 980-5 Kwan-yang Dong, Anyang City, S. Korea) (0.30 mmol) dissolved in 10 mL of dichloromethane. The resulting solution was stirred at room temperature overnight. The solvent was evaporated under vacuum and the resulting polymer was precipitated with ether.

Example 11

10 Synthesis of triadamantane crosslinker:

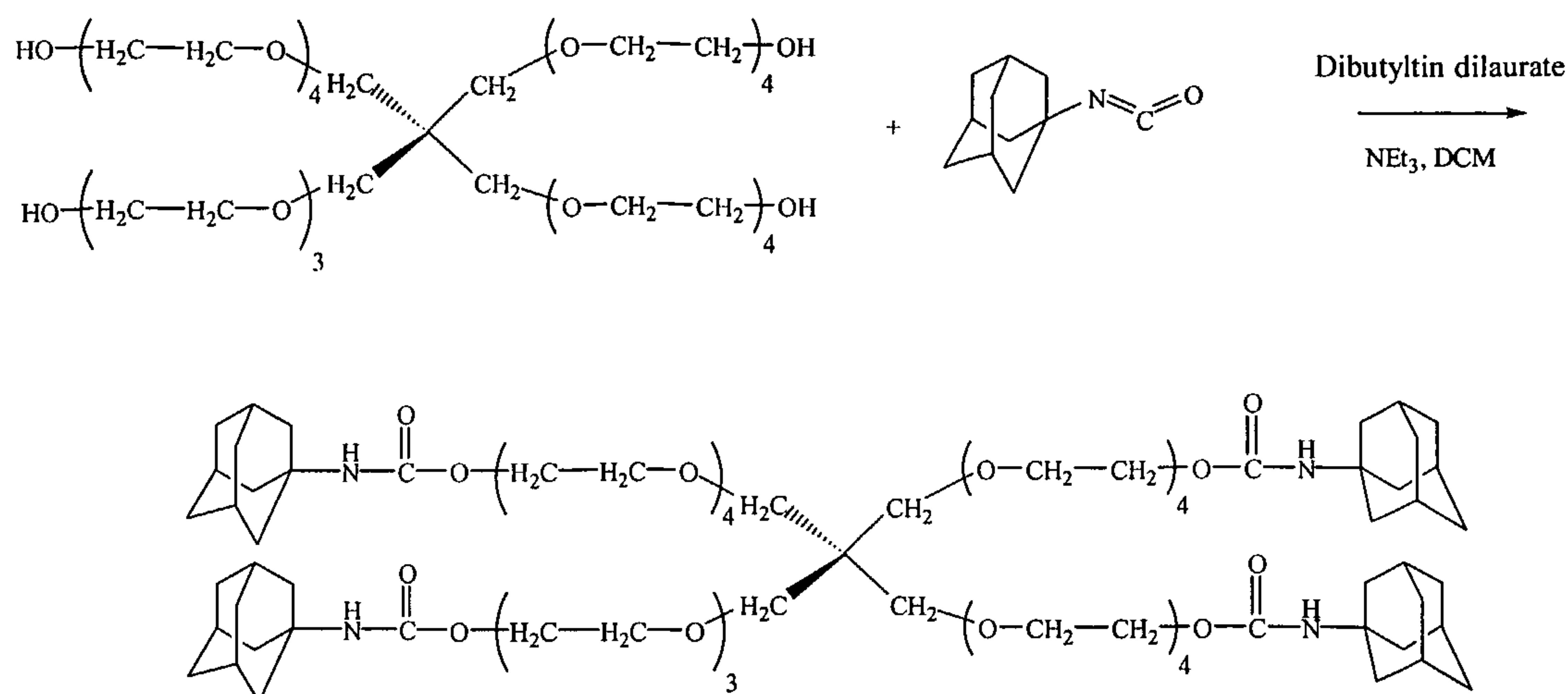


1-Adamantanemethylamine (0.212 g, 1.29 mmol, Aldrich, Milwaukee, WI) was added to Tris-succinimidyl aminotriacetate (TSAT) (0.2 g, 0.41 mmol, Pierce, Rockford, IL) dissolved in 10 mL of anhydrous dimethylformamide (Aldrich, Milwaukee, WI). The resulting mixture was stirred at room temperature under argon for 14 h. The precipitated was filtered and characterized by mass spectroscopy: Electrospray Ionization: 633.4 [M+H]⁺, 655.6 [M+Na]⁺, 1265.3 [2M+H]⁺, 1287.1 [2M+Na]⁺.

Example 12*Synthesis of tetraadamantane crosslinker:*

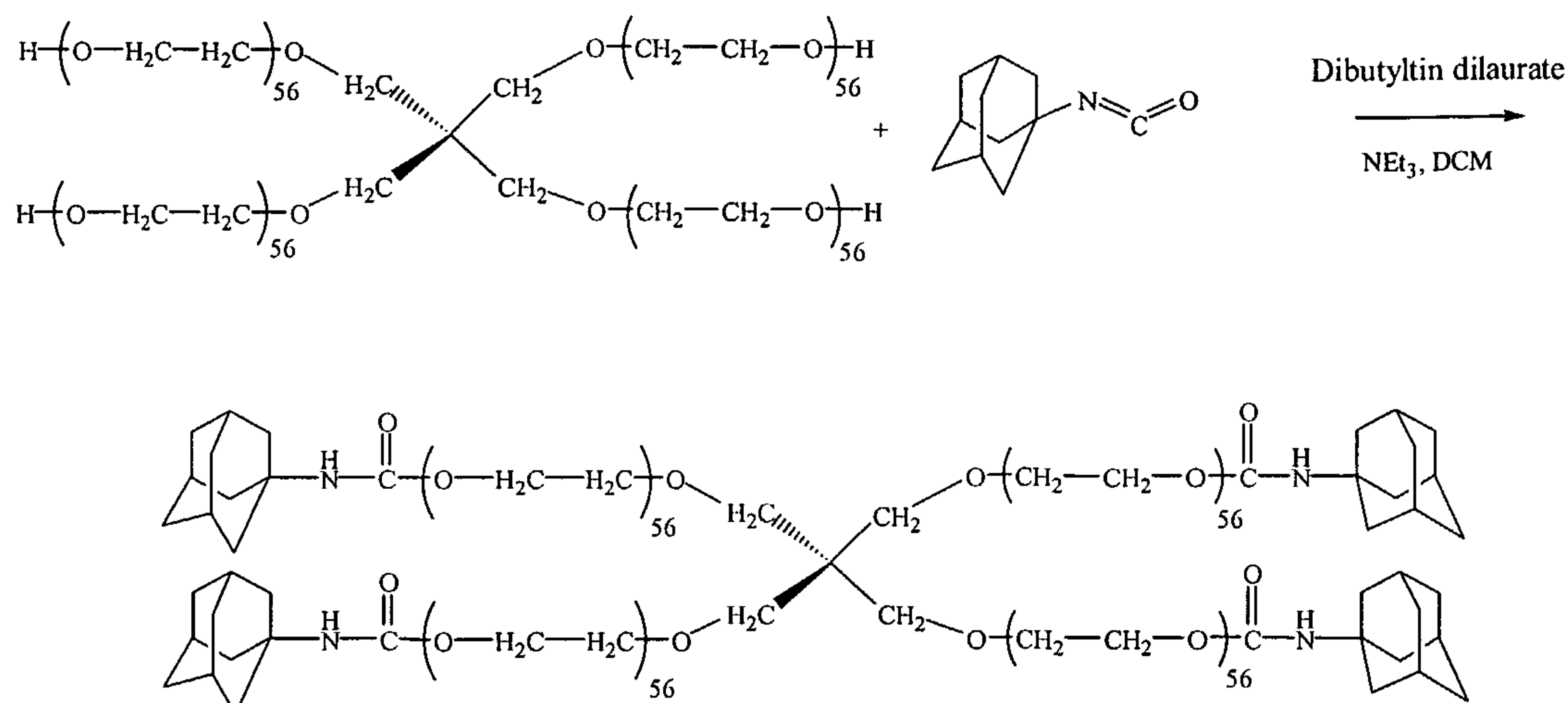
1-Adamantanemethylamine (0.212 g, 1.29 mmol, Aldrich, Milwaukee, WI) was
 5 added to Tetrakis-(N-succinimidylcarboxypropyl)pentaerythritol (NHS-4) (0.1 g,
 0.12 mmol, Molecular Biosciences, Boulder, CO) dissolved in 5 mL of anhydrous
 dimethylformamide (Aldrich, Milwaukee, WI). The resulting mixture was stirred at
 room temperature under argon for 14 h. The precipitated was filtered and
 characterized by Mass Spectroscopy: Electrospray Ionization: 1013.7 $[M+H]^+$,
 10 1035.8 $[M+Na]^+$.

Example 13*Synthesis of tetra-adamantane polyethylene glycol crosslinker:*Method I: Using pentaerythritol ethoxylate (15/4 EO/OH)



Pentaerythritol ethoxylate (15/4 EO/OH) (Mn = 797) (1mmol, Aldrich, Milwaukee, WI) is dried by heating under vacuum at 70 °C overnight. 1-Adamantyl isocyanate (4.4 mmol, Aldrich, Milwaukee, WI) is added to the dried polymer after its dissolution in anhydrous dichloromethane (25 mL). Two catalysts, dibutyltin dilaurate (0.1 mmol, Aldrich, Milwaukee, WI) and triethylamine (0.1 mmol, Aldrich, Milwaukee, WI) are then added. The reaction mixture is heated under reflux for 7 hours. After removal of the solvent, the reaction product is dissolved in distilled water. The aqueous solution is purified by addition of activated carbon and successive filtrations, and then freeze-dried.

Method II: Using 4 arm PEG



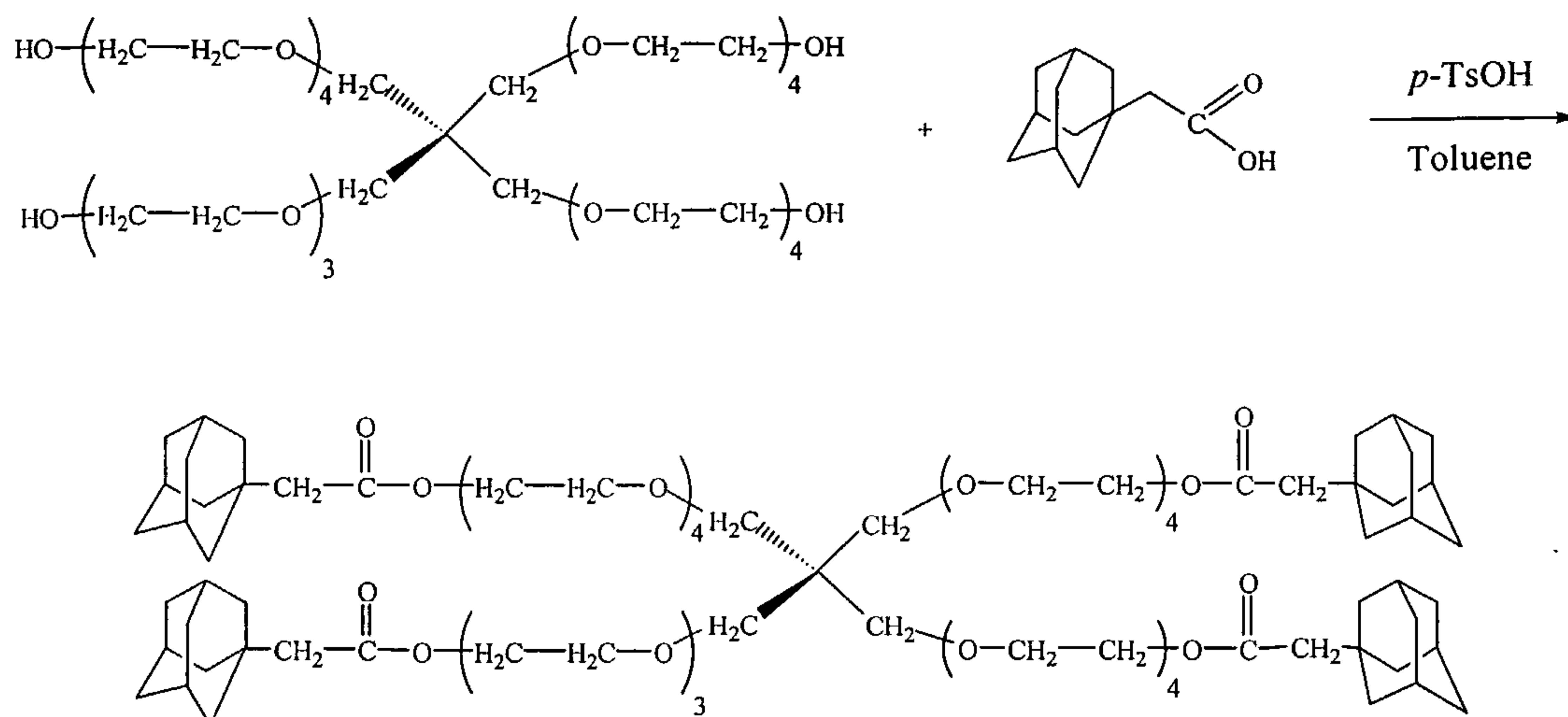
4 arm PEG (Mn = 10000) (1mmol, Shearwater Polymers, Inc, Huntsville, AL) is dried by heating under vacuum at 70 °C overnight. 1-Adamantyl isocyanate (4.4 mmol, Aldrich, Milwaukee, WI) is added to the dried polymer after its dissolution in anhydrous dichloromethane (25 mL). Two catalysts, dibutyltin dilaurate (0.1 mmol, Aldrich, Milwaukee, WI) and triethylamine (0.1 mmol, Aldrich, Milwaukee, WI) are then added. The reaction mixture is heated under reflux for 7 hours. After removal of the solvent, the reaction product is dissolved in distilled water. The aqueous solution is purified by addition of activated carbon and successive filtrations, and then freeze-dried.

Example 14

Synthesis of hydrolysable tetra-adamantane polyethylene glycol crosslinker:

15

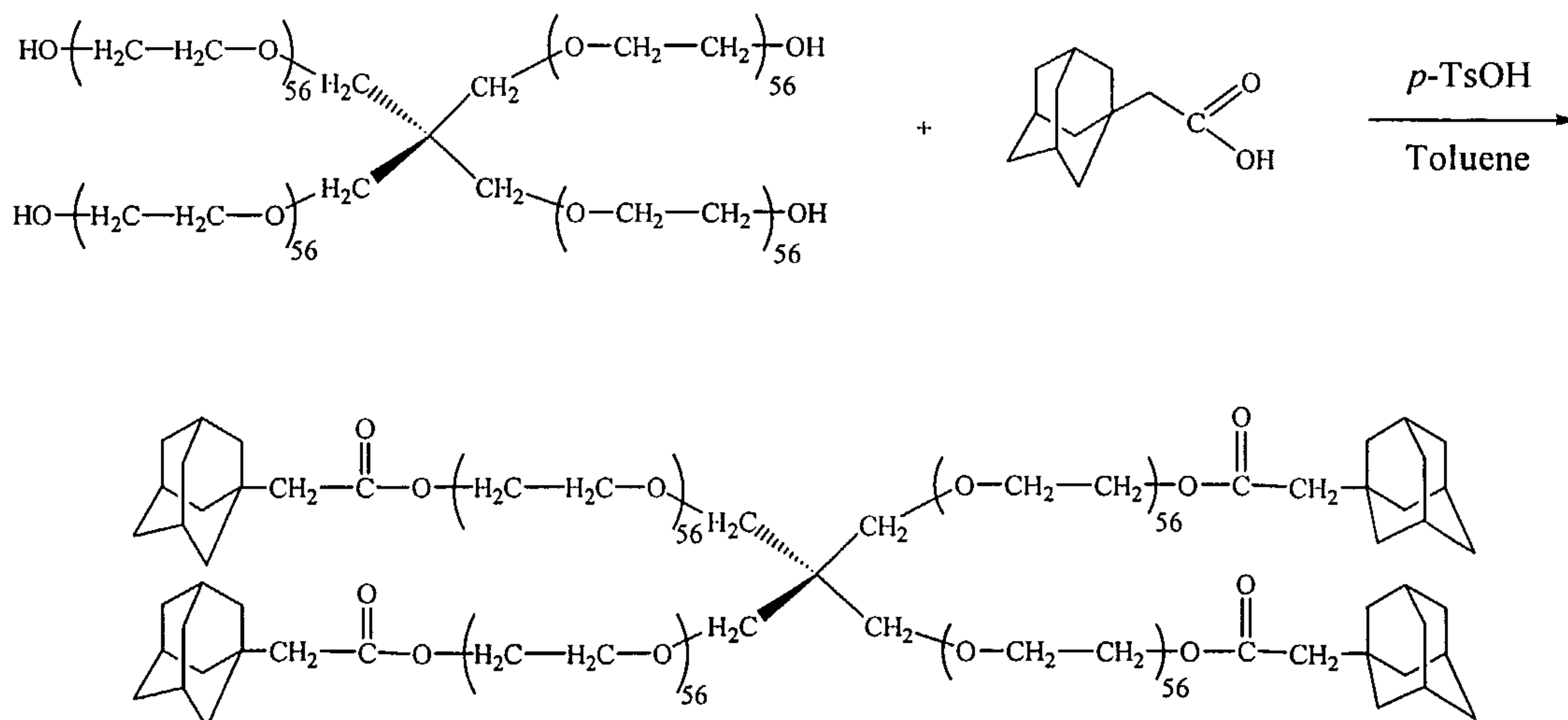
Method I: Using pentaerythritol ethoxylate (15/4 EO/OH)



Pentaerythritol ethoxylate (15/4 EO/OH) ($M_n = 797$) (1mmol, Aldrich, Milwaukee, WI) is dried by heating under vacuum at 70 °C overnight. 1-Adamantaneacetic acid (4.4 mmol, Aldrich, Milwaukee, WI) is added to the dried polymer after its dissolution in anhydrous toluene. p -Toluenesulfonic acid (Aldrich, Milwaukee, WI) is then added in a catalytic amount. The resulting mixture is azeotropically refluxed for 16 h using Dean-Stark apparatus. After completion of the reaction, the solvent is removed under vacuum and the resulting polymer is precipitated with ether.

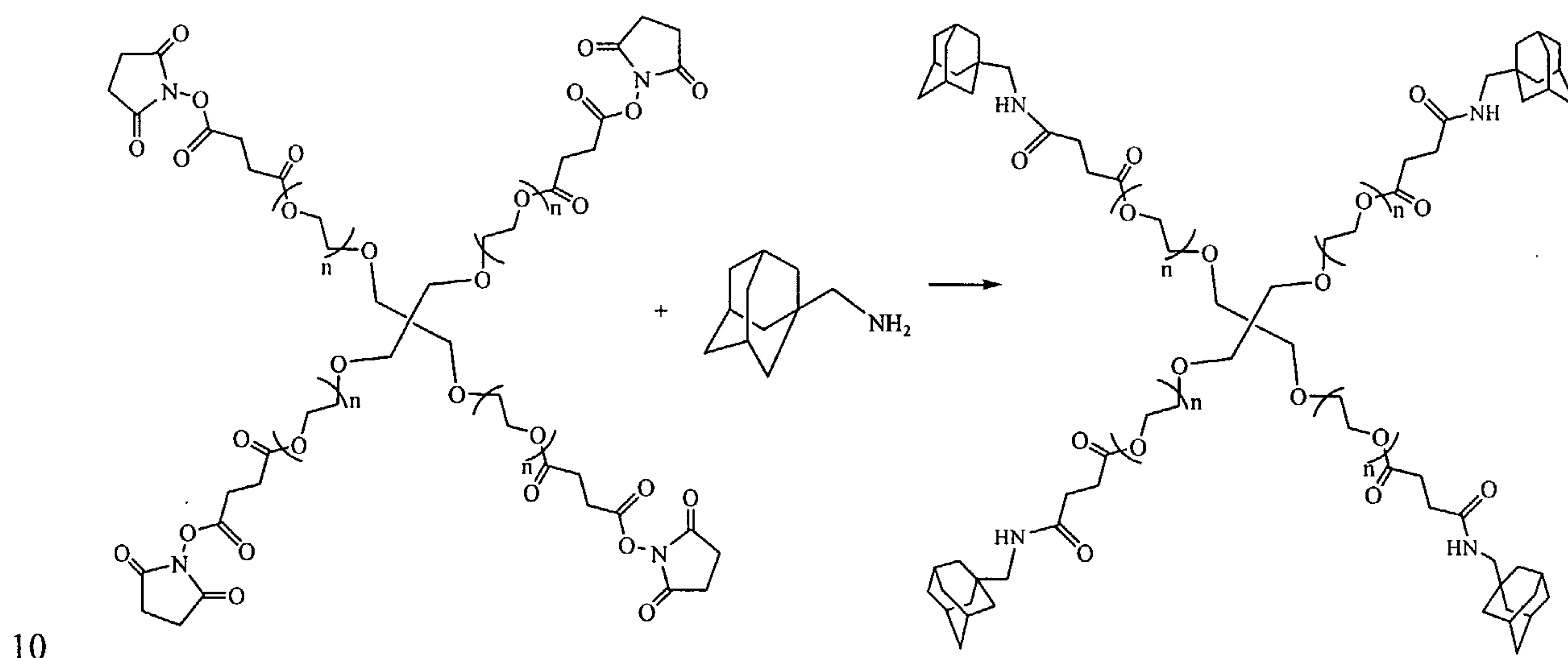
10

Method II: Using 4 arm PEG



4 arm PEG ($M_n = 10000$) (1 mmol, Shearwater Polymers, Inc, Huntsville, AL) is dried by heating under vacuum at 70 °C overnight. 1-Adamantaneacetic acid (4.4 mmol, Aldrich, Milwaukee, WI) is added to the dried polymer after its dissolution in anhydrous toluene. *p*-Toluenesulfonic acid (Aldrich, Milwaukee, WI) is then added in a catalytic amount. The resulting mixture is azeotropically refluxed for 16 h using Dean-Stark apparatus. After completion of the reaction, the solvent is removed under vacuum and the resulting polymer is precipitated with ether.

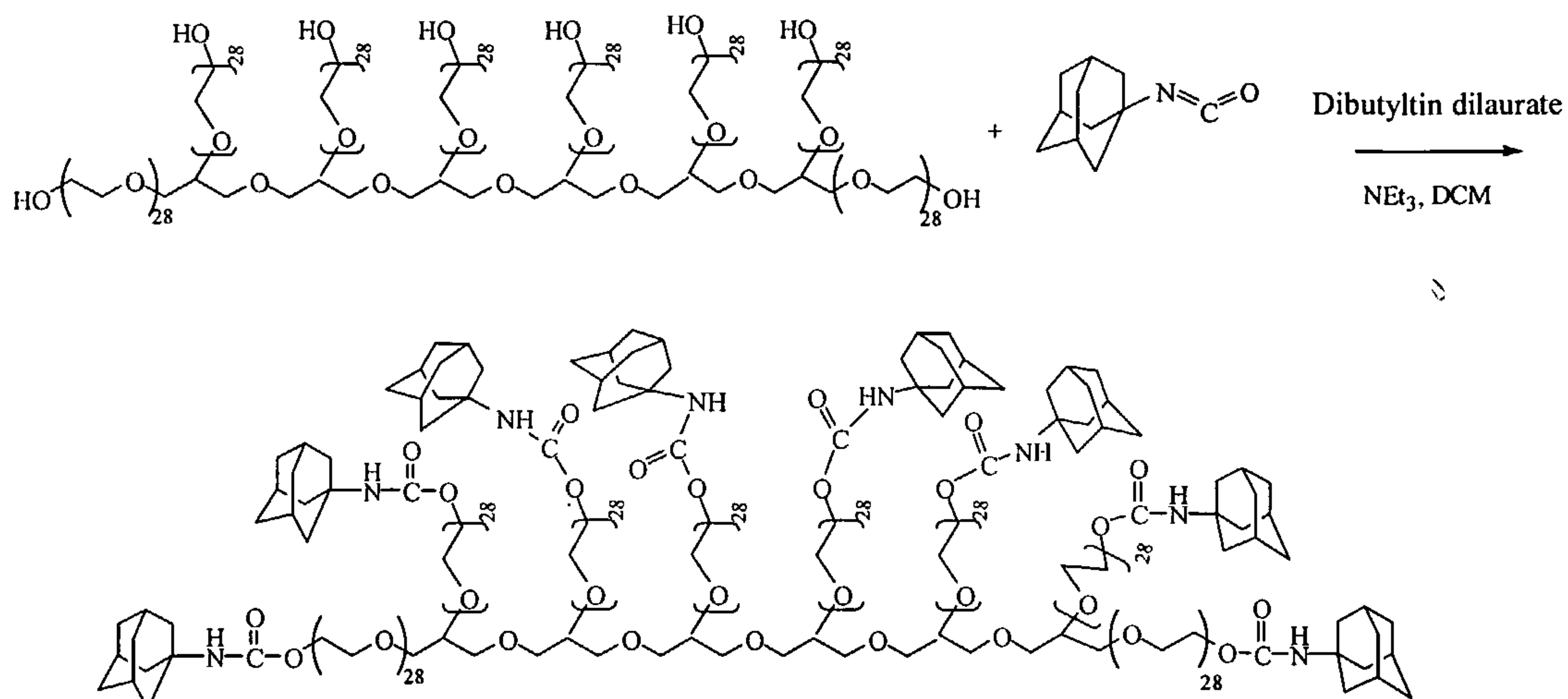
Method III: Using 4-arm PEG-succinimidyl succinate (PEG-SS)₄



1-Adamantanemethylamine (0.069 g, 0.44 mmol, Aldrich, Milwaukee, WI) was added to 1 g of disuccinimidyl succinate polyethylene glycol ((PEG_{10k}-SS)₄) (SunBio, Inc., 980-5 Kwan-yang Dong, Anyang City, S. Korea) (0.1 mmol) previously dissolved in 10 mL of dichloromethane. The resulting solution was stirred at room temperature overnight. The solvent was evaporated under vacuum and the resulting polymer was precipitated with ether.

Example 15

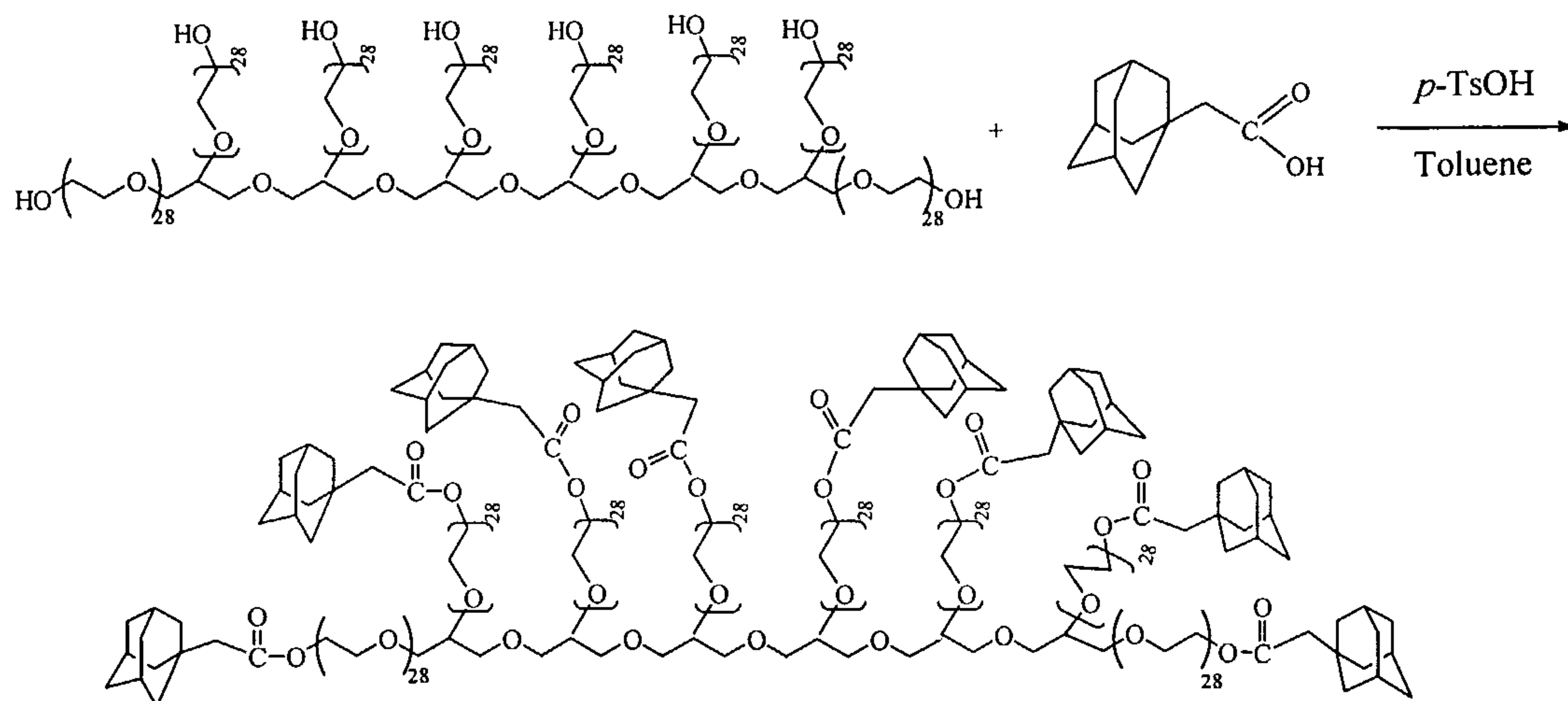
Synthesis of octa-adamantane polyethylene glycol crosslinker:



8 arm PEG (Mn = 10000) (1mmol, Shearwater Polymers, Inc, Huntsville, AL) is dried by heating under vacuum at 70 °C overnight. 1-Adamantyl isocyanate (4.4 mmol, Aldrich, Milwaukee, WI) is added to the dried polymer after its dissolution in anhydrous dichloromethane (25 mL). Two catalysts, dibutyltin dilaurate (0.1 mmol, Aldrich, Milwaukee, WI) and triethylamine (0.1 mmol, Aldrich, Milwaukee, WI) are then added. The reaction mixture is heated under reflux for 7 hours. After removal of the solvent, the reaction product is dissolved in distilled water. The aqueous solution is purified by addition of activated carbon and successive filtrations, and then freeze-dried.

Example 16

Synthesis of hydrolysable octa-adamantane polyethylene glycol crosslinker:



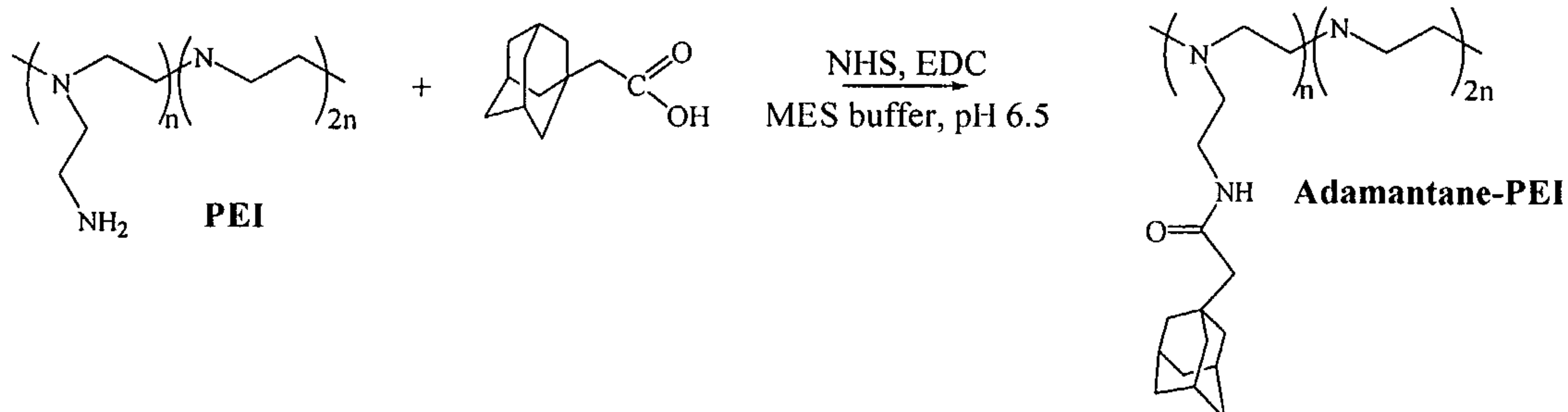
8 arm PEG ($M_n = 10000$) (1mmol, Shearwater Polymers, Inc, Huntsville, AL) is dried by heating under vacuum at 70 °C overnight. 1-Adamantaneacetic acid (4.4 mmol, Aldrich, Milwaukee, WI) is added to the dried polymer after its dissolution in anhydrous toluene. p -Toluenesulfonic acid (Aldrich, Milwaukee, WI) is then added in a catalytic amount. The resulting mixture is azeotropically refluxed for 16 h using Dean-Stark apparatus. After completion of the reaction, the solvent is removed under vacuum and the resulting polymer is precipitated with ether.

10

Example 17

Synthesis of multi adamantane crosslinker:

Method I: Using branched PEI

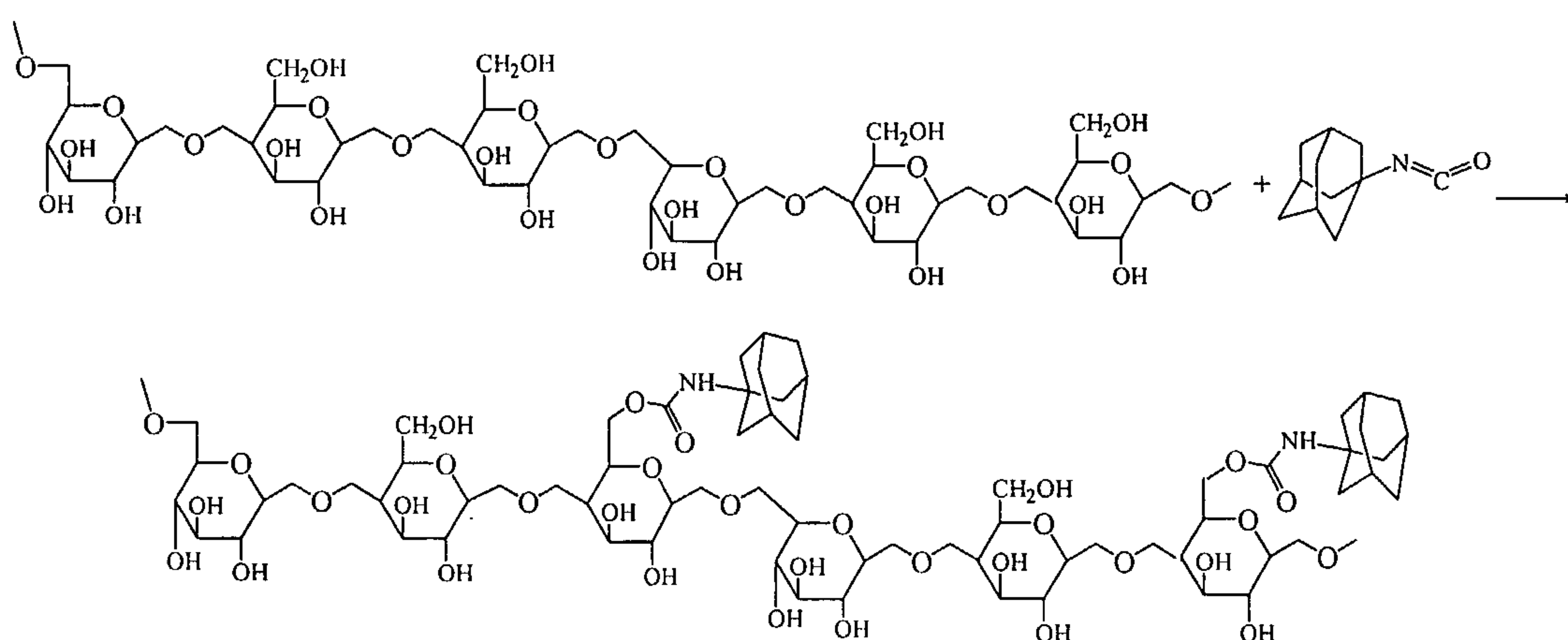


15

1-Adamantaneacetic acid (Aldrich, Milwaukee, WI) is added to PEI (Aldrich, Milwaukee, WI) dissolved in MES buffer 25 mM, pH 6.5. 1-(3-dimethylaminopropyl)-3-ethylcarbodiimide hydrochloride (EDC) (Aldrich, Milwaukee, WI) and N-Hydroxysuccinimide (NHS) (Aldrich, Milwaukee, WI) are then added to the reaction mixture. The reaction mixture is stirred at room temperature for 24 h and then transferred to a 10000 MWCO Spectra/Por membrane and dialyzed against water for 24 h. The solution was then freeze-dried to dryness.

Method II: Using pullulan

10 (Akiyoshi et al. 1993, Macromolecules 26:3062-3068)

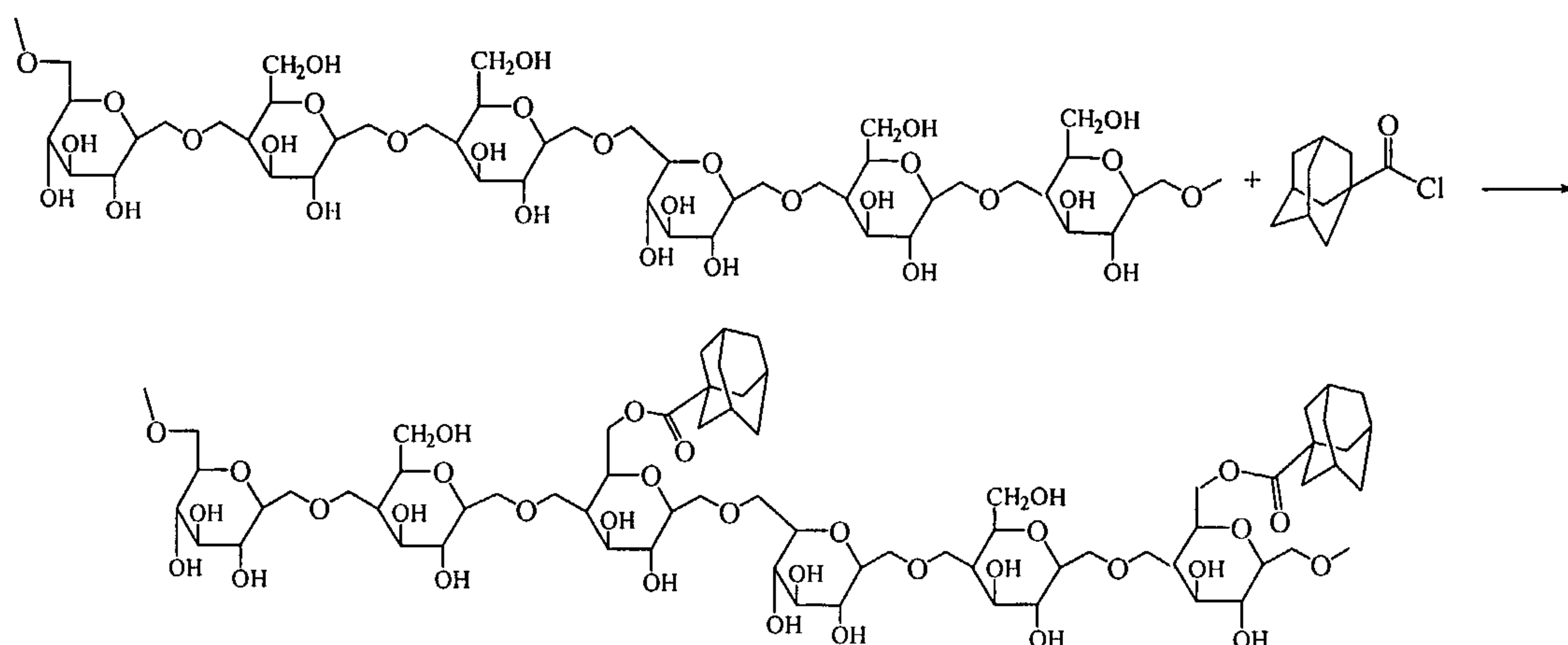


1-Adamantyl isocyanate (Aldrich, Milwaukee, WI) is reacted with Pullulan (Sigma-Aldrich, Milwaukee, WI) in anhydrous DMSO containing pyridine at 80 °C for 8 h. Ethanol is added to the reaction mixture, and the resulting mixture is stored overnight at 4 °C. The precipitates are separated, purified by dialysis against water and lyophilized to dryness. The degree of substitution of the adamantane group is determined by ¹H NMR.

20 **Example 18**

Synthesis of hydrolysable multi adamantane crosslinker:

(Sunamoto et al. 1992, Macromolecules 25:5665-5670)



Pullulan (Sigma-Aldrich, Milwaukee, WI) is dissolved in anhydrous DMF at 60 °C. 1-Adamantanecarbonyl chloride (Aldrich, Milwaukee, WI) dissolved in anhydrous DMF and anhydrous Pyridine are added. The resulting mixture is stirred at 60 °C for 2 h and another 1 h at room temperature. The mixture is poured into ethanol. The precipitates are collected and washed with ethanol and then, with diethyl ether. The solid is dried under vacuum at 50 °C for 2 h. The degree of substitution of the adamantane group is determined by ¹H NMR.

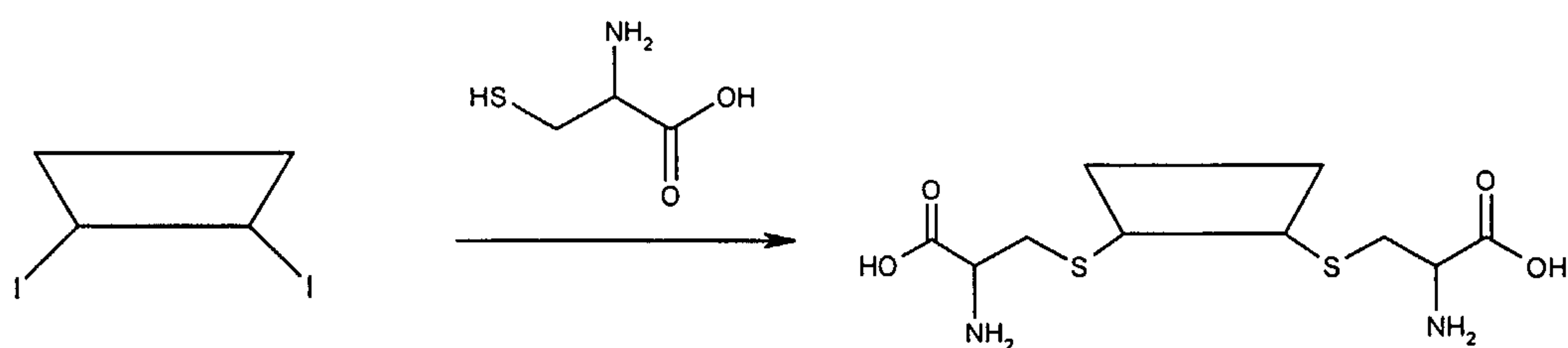
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Example 19

Synthesis of self-crosslinked polymer:

The synthesis of a polymer that contains cyclodextrin and adamantane functions is carried out in three steps.

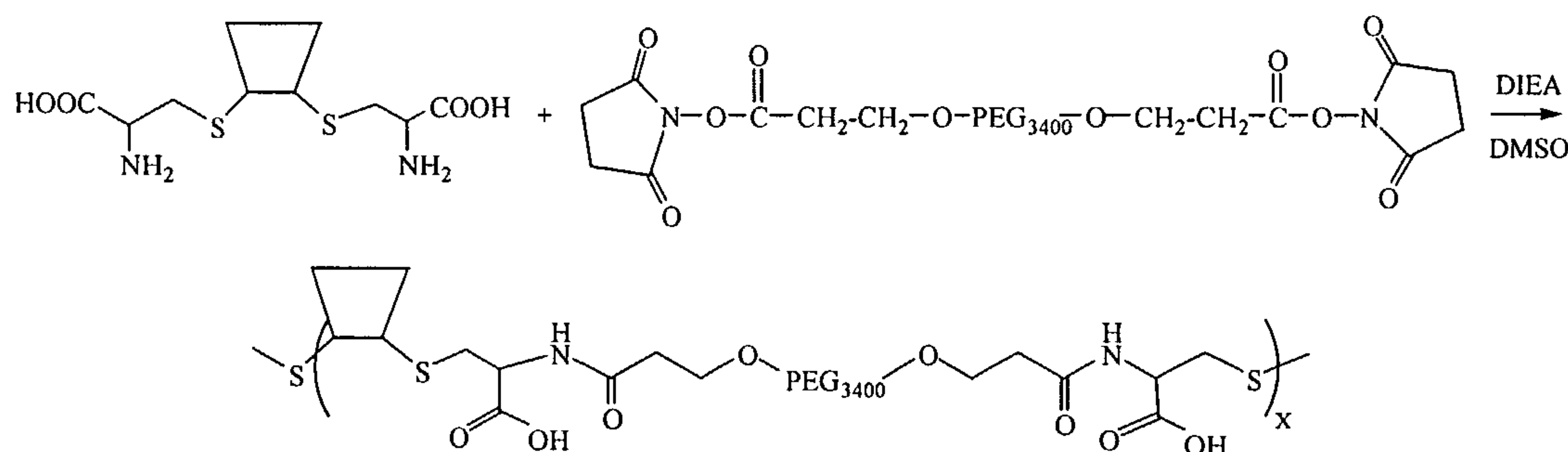
1. Step 1: Synthesis of monomer 6^A,6^D-Bis-(2-amino-2-carboxylethylthio)-6^A,6^D-dideoxy-β-cyclodextrin, (CD-BisCys)



A 167 mL of 0.1 M sodium carbonate buffer was degassed for 45 minutes in a 500 mL 2-neck round bottom flask equipped with a magnetic stir bar, a condenser and septa. To this solution was added 1.96 g (16.2 mmol) of L-cysteine and 10.0 g (73.8 mmol) of di-iodo- β -cyclodextrin (Gonzalez et al. 1999 Bioconjugate Chem. 10:1068-1074; and Hwang et al. 2001 Bioconjugate Chem. 12(2): 280-290; Gonzalez, H., Hwang, S.J., and Davis, M.E. (2000) Linear Cyclodextrin Copolymers WO001734A1). The resulting suspension was heated at a reflux temperature for 4.5 h. until the solution turned clear colorless. Then, it was cooled to room temperature and acidified to pH 3 using 1 N HCl. The product was crashed out by slow addition of acetone (3 times weight ratio of the solution). This afforded 9.0 g (90.0%) yield of CD-BisCys. The resulting solid was subjected to anionic exchange column chromatography using a gradient elution of 0-0.4 M ammonium bicarbonate solution. ESI/MS (m/z): 1342 $[M]^+$, 1364 $[M + Na]^+$. Purity of CD-BisCys was confirmed by HPLC.

15

2. Step 2: Synthesis of CD-BisCys-PEG₃₄₀₀ Copolymers



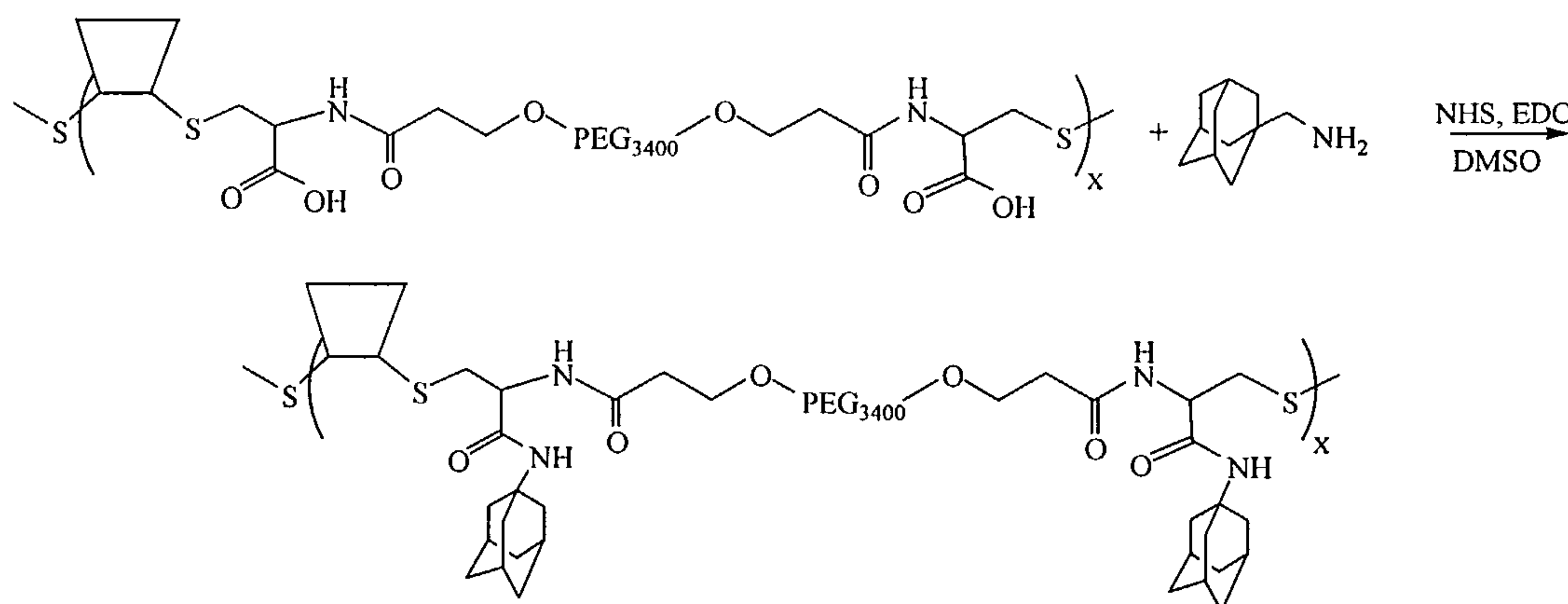
CD-BisCys (2 g, 1.49 mmol) and SPA-PEG₃₄₀₀-SPA (5.07 g, 1.49 mmol, Shearwater Inc.) were dissolved in dry DMSO (40 mL). After 10 minutes diisopropylethylamine (DIEA, 0.571 mL, 2.2 eq, Aldrich) was added under argon. The reaction mixture was stirred under argon for 2-6 days. An increase of viscosity was observed as a function of polymerization time. Water (200 mL) was added to the polymerization solution with vigorous stirring. The solution was then dialyzed in 25,000 MWCO Spectra/Por 7 membrane for 2.5 days at a concentration of ca. 10

mg polymer/mL water. After lyophilization, a white fluffy powder (6.2 g, 92% yield) was obtained.

Characterization: Light Scattering and Molecular Weight Determination

The specific refractive index increment, dn/dc , was measured in Phosphate Buffered Saline 1x (PBS) (Cellgro, Mediatech, Inc, Herndon, VA) using a Bausch & Lomb ABBE-3L refractive index. Polymer samples were then analyzed on a Hitachi D6000 HPLC system equipped with a ERC-7512 RI detector, a Precision Detectors PD2020/DLS static light scattering detector and an PL aquagel-OH 30 (Polymer Laboratories, Amherst, MA) column using Phosphate Buffered Saline 1x as eluant at a 0.7 mL/min flow rate. The dn/dc was calculated to be 0.1348 and the weight average molecular weight M_w was determined to be 103,500 Da with a polydispersity index M_w/M_n of 1.71.

3. Adamantane conjugation to CD-BisCys-PEG₃₄₀₀ Copolymers



15

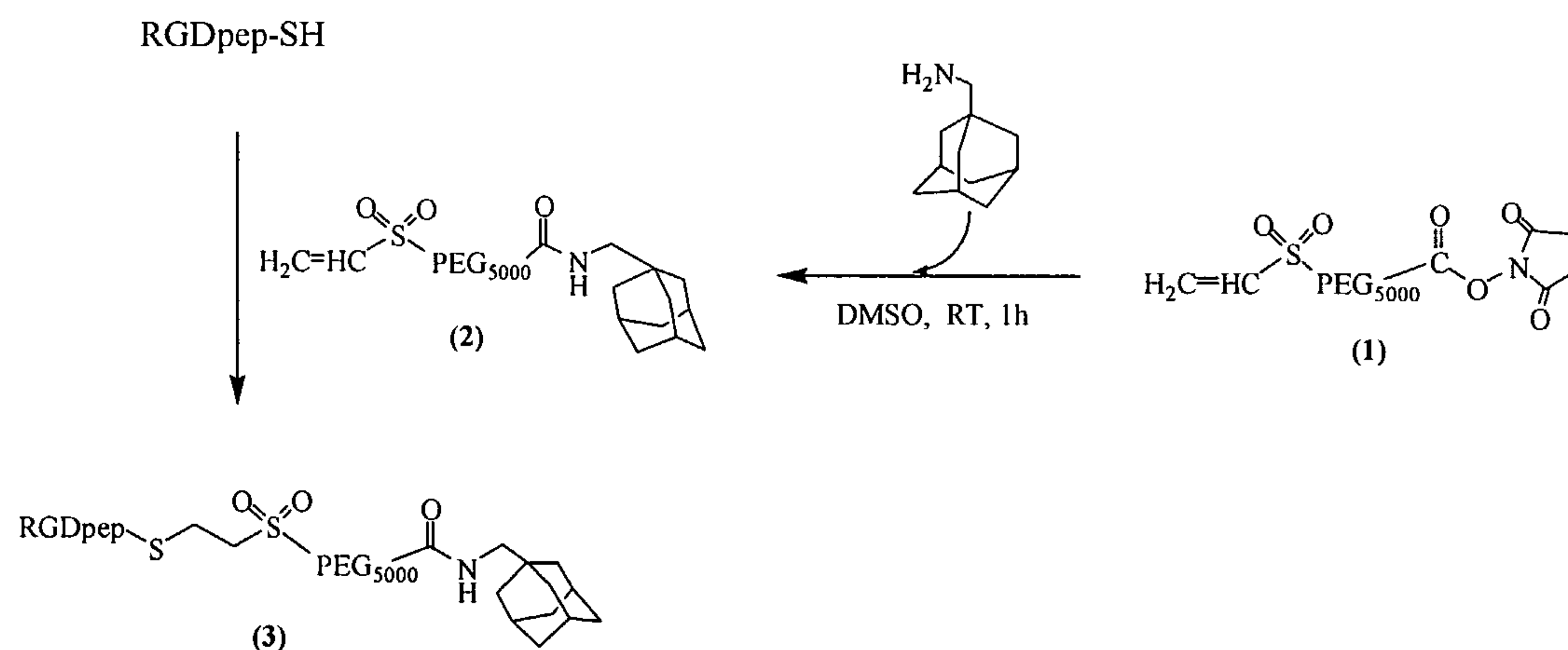
CD-BisCys-PEG₃₄₀₀ copolymer (0.32 mmol of repeat unit) is dissolved in dry DMSO and stirred for 10 minutes. 1-Adamantanemethylamine (0.76 mmol, Aldrich, Milwaukee, WI), DIEA (0.76 mmol), EDC (0.96 mmol) and NHS (0.71 mmol) are added to the polymer solution. The mixture is stirred for about 16 hours. Water is added to the resulting mixture to remove excess 1-Adamantanemethylamine. After filtration of the precipitates, the solution is dialyzed against water with

20

10,000 MWCO Spectra/Por membrane for 48 h and lyophilized to dryness. The degree of substitution of the adamantane group is determined by ^1H NMR.

Example 20

5 *Synthesis of RGD-modified Adamantane-PEG derivative*



Step 1: Synthesis of VS-PEG₅₀₀₀-AD (2)

- 10 Vinylsulfone-PEG₅₀₀₀-NHS (1) (Shearwater Polymers, 0.147 mmol) was added to a round bottom flask equipped with a stir bar and dissolved in 5 mL of DMSO. To this was added Adamantanemethylamine (Aldrich, 0.147 mmol). The resulting solution was stirred 1 h at room temperature. The resulting mixture was dialyzed overnight against 3500 MWCO Membrane (Spectra Por). The solution was
- 15 then lyophilized to afford Vinylsulfone-PEG₅₀₀₀-AD (2).

Step 2: RGDpep-PEG-AD conjugate synthesis

- RGDpep-SH synthesized as described in Kok et al. (Bioconjugate Chemistry (2002), 13(1), 128-135) is dissolved in PBS (phosphate buffer saline) 1x, pH 7.2.
- 20 Vinylsulfone-PEG₅₀₀₀-AD (2) is then added to the RGDpep-SH solution. The resulting solution is stirred at room temperature for 2 hours. The polymer solution is then transferred to a Spectra/Por 7 MWCO 3500 membrane (Spectrum, Houston,

TX) and dialyzed against water for 24 h. The solution is then freeze-dried to dryness to afford RGDpep-PEG₅₀₀₀-AD (3).

Example 21

Preparation of material:

- 5 The polymer bearing the inclusion host (Example 1-6) was dissolved at 100 mg/mL in PBS (phosphate-buffered saline) 1x, pH 7.2. The crosslinker (Example 7-18) (ratio: Adamantane/cyclodextrin: 1/1 or 1/2) was then added. The resulting mixture was mixed vigorously in order to get the crosslinker in solution. An increase in the viscosity was observed in about 10 min.

10 Example 22

Preparation of ionic type material:

Using multivalent ion

- The polymer bearing the inclusion host and carboxyl groups (See Example 19, Step 2) was dissolved at 100 mg/mL in 0.1 M CaCl₂ aqueous solution and then
15 added to a vial containing a mixture of the crosslinker (Example 7-18) (ratio: Adamantane/cyclodextrin: 1/1 or 1/2). The resulting mixture was mixed vigorously in order to get the crosslinker and the diamino compound in solution. An increase in the viscosity was observed.

Using diamino compound

- 20 The polymer bearing the inclusion host and carboxyl groups (See Example 19, Step 2) was dissolved at 100 mg/mL in water and then added to a vial containing a mixture of the crosslinker (Example 7-18) (ratio: Adamantane/cyclodextrin: 1/1 or 1/2) and a diamino compound like PEG₃₄₀₀-(NH₂)₂ (Shearwater Polymers) or C_nH_{2n}-(NH₂)₂ (ratio: NH₂/COO⁻: 1/1 or 1/2). The resulting mixture was mixed vigorously
25 in order to get the crosslinker and the diamino compound in solution. An increase in the viscosity was observed.

Using polycation

The polymer bearing the inclusion host and carboxyl groups (See Example 19, Step 2) was dissolved at 100 mg/mL in water and then added to a vial containing a mixture of the crosslinker (Example 7-18) (ratio: Adamantane/cyclodextrin: 1/1 or 1/2) and a polycation like polylysine or polyethyleneimine. The resulting mixture
5 was mixed vigorously in order to get the crosslinker and the polycation in solution. An increase in the viscosity was observed.

Example 23

Preparation of material containing virus or protein:

The polymer bearing the inclusion host (Example 1-6) was dissolved in PBS
10 (phosphate-buffered saline) 1x, pH 7.2 containing the protein or virus at the desired concentration to obtain a polymer solution at a final concentration of 100 mg/mL of solution. The crosslinker (Example 7-18) (ratio: Adamantane/cyclodextrin: 1/1 or 1/2) was then added. The resulting mixture was mixed vigorously in order to get the crosslinker in solution. An increase in the viscosity was observed in about 10
15 min.

Example 24

Preparation of material containing a signaling peptide

The polymer bearing the inclusion host (Example 1-6) is dissolved in PBS (phosphate-buffered saline) 1x, pH 7.2 (containing when desired proteins, virus, or
20 other drugs or drug delivery systems) at the desired concentration to obtain a polymer solution at a final concentration of 100 mg/mL of solution. The crosslinker (Example 7-18) (ratio: Adamantane/cyclodextrin: 1/2) and the signaling peptide (Example 20) (ratio: Adamantane/cyclodextrin: 1/2) are then added. The resulting mixture is mixed vigorously in order to get the crosslinker in solution. An increase
25 in the viscosity is observed in about 10 min.

Example 25

Studies concerning cell mobility through matrix.

- a. Matrix (0.2 mL, composed of CD-PEG₃₄₀₀ and bis-(2(1-adamantyl)ethyl)phosphate) was prepared as described in Example 21 and added to the bottom of FluoroBlok inserts (for 24 well format, Falcon Catalog #351152).
- 5 b. CCD cells were rinsed with PBS and then exposed to 5 μ M of Calcein-AM, a fluorescent marker, for 15-30 minutes.
- c. CCD cells were then trypsinized and plated on top of the matrix in the insert at 10,000 cells/insert in 0.5 mL media.
- d. 1 mL of media containing 10 ng/mL human PDGF protein was then
10 added to the lower chamber.
- e. Cell mobility through the matrix and into the lower chamber was monitored for 3 days by fluorescence microscopy. Successful migration through the matrix and past the insert was demonstrated by the presence of cells in the lower chamber observed by fluorescence microscopy
15 hours after plating as shown in Figure 5.

Example 26

Transfection studies to CCD fibroblast cells with CD-PEI polyplexes formulated with matrix.

- 20 The well bottoms in 24-well plates were coated with ~0.2 mL of the following:
- a. No coating (control)
 - b. Matrix
 - c. Matrix containing 1 μ g of luciferase gene-containing plasmid.
 - 25 d. Matrix containing CDP polyplex.
 - e. Matrix containing CDPEI polyplex.
 - f. No coating. Free CDPEI polyplex (positive control I: traditional transfection procedure)
 - g. No coating. Free CDP polyplex (positive control II: traditional
30 transfection procedure).

CCD (fibroblast cells, ATCC) were plated in the 24 well plates at 40,000 cells/well. 24 hours after plating the cells, media was removed, cells rinsed with PBS, and lysed. The cell lysates were analyzed for luciferase protein activity using
5 luciferase assay. Results are reported in RLU/well. This experiment demonstrates that the cells are able to successfully migrate into the matrix and be transfected by the polyplexes contained in the matrix. Transfection efficiency is only slightly lower than transfection by polyplexes free in media.

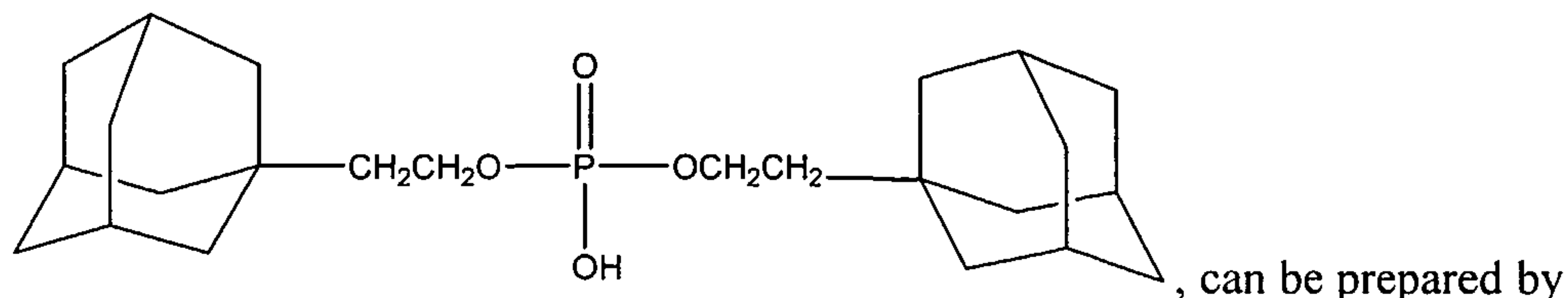
Note: the matrix is comprised of CD-PEG (see Example 3, method II for
10 synthesis procedure) crosslinked with a diadamantane crosslinker (bis-(2(1-adamantyl)ethyl)phosphate, see Example 7 for synthesis procedure). Matrix formulation procedure is described in Example 21. When polyplexes are included in the matrix, the polyplexes are prepared by adding a 10 μ L solution of polymer to 10 μ L solution of luciferase gene-containing plasmid (0.1 mg/mL) at the optimum
15 charge ratio. The polyplexes are included in the buffer solution that is used to dissolve the CD-PEG component of the matrix and matrix formulated as described in Example 21.

For positive control experiments, polyplexes are prepared as described and added directly to the cell media.

20 **Example 27**

Materials can be prepared, as schematically depicted in Figure 1, by the self-assembly of cyclodextrin (CD)-containing polymers (**A**) and di- or multi-functional linkers (**B**) terminated with molecules capable of forming inclusion complexes with the cyclodextrin-containing polymers. The materials (**P**) may be formulated to
25 contain proteins, cells, viruses, polyplexes, or other therapeutic agents or delivery systems containing therapeutic agents.

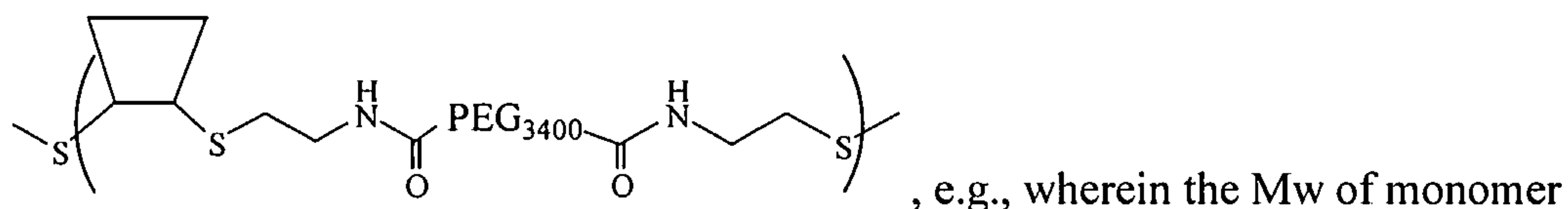
An exemplary linker,



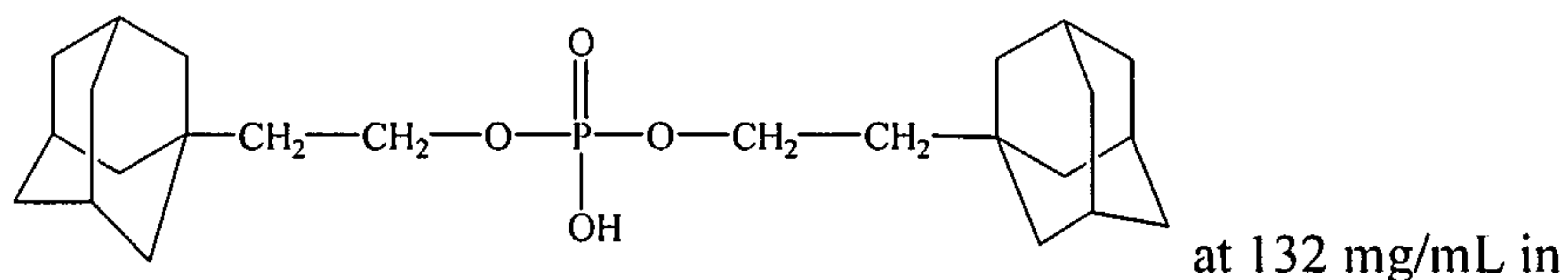
following the protocols described in the Breslow and Zhang, JACS (1996), 118, 8495-8496, and Zhang and Breslow, JACS (1993), 115, 9353-9354. One of skill in the art can readily modify this protocol, in light of techniques generally known in the art, to arrive at a wide spectrum of different linkers that can be employed as linking molecules as the term is used herein. The difunctional linkers or cyclodextrin-containing polymers may contain biodegradable linkages to facilitate the release of the therapeutic agents and/or degradation of the material.

Compounds increasing the therapeutic utility of the material, such as signaling peptides or other moieties facilitating cell migration, may be incorporated into the material by conjugating a inclusion complex guest to the entity of interest and including the conjugate in the material as described in Figure 2. The conjugate may be included before, during or after the crosslinking process.

For example, a polymer made of repeated subunits having the formula:



is approximately 4800, can be prepared as a solution of the polymer at 100 mg/mL in PBS (phosphate-buffered saline) 1x, pH 7.2. It may be desirable to centrifuge the mixture and then agitate the solution to solubilize the polymer. A 33.3 μ L aliquot of a solution of the linking molecule



dichloromethane, can be placed into a vial to let the dichloromethane evaporate at room temperature or in an oven at 37 °C. 1 mL of the polymer solution can then be

added to the residual linker, optionally triturating to facilitate solution. The solution may then be allowed to rest, and after a time, e.g., 10 min., the solution may become viscous. To include a foreign substance, such as a therapeutic agent or viral particles, into the crosslinked polymer, the substance may be present in the solution prior to the final resting period. For example, the substance may be present in the solvent used to dissolve the cyclodextrin polymer or in the initial solution of the linking molecule, or may be added to either component or to the final solution prior to the crosslinking reaction.

Example 28

10 Methods and Results:

Matrix 1 (60 kD polymer prepared according to Example 3, method II and crosslinking agent prepared according to Example 9, method II) and Matrix 2 (80 kD polymer prepared according to Example 3, method II and crosslinking agent prepared according to Example 9, method II) were used.

15 Application of 60kD matrix in vivo.

300 μ l of 60 kD matrix was drawn up into a 1 cc syringe and all air bubbles were removed by moving the syringe plunger up and down. A 23G needle was large enough for matrix to pass through with some pressure required. A 20G needle was large enough to allow the matrix to pass through easily.

20 Male Sprague-Dawley rats were sacrificed, shaved, and 8 mm wounds were made on their dorsal regions. Using a 1 cc syringe with 20G needle, excess 60 kD matrix was expelled until 100 μ L of volume remained. Matrix was then applied to an 8 mm wound punch without any over-fill. The same procedure was performed except with 150 μ l of Matrix 1 and this over-filled an 8 mm punch wound in rat
25 dorsum skin.

The feasibility of applying matrix to an incisional wound was explored. A full-thickness incision approximately 2 inches in length was made on a rat dorsum.

A syringe was filled with 200 μ L of 60 kD matrix and was successfully injected intra-dermally at the incision site using a 20G needle.

Application of 80kD matrix

Two 8 mm full-thickness dermal punches were made on a rat dorsum. One
5 punch was treated with 100 μ L of 80 kD matrix using a 1 cc syringe and a 20G needle. This volume filled the punch evenly; however, more force was required to deliver 80 kD when compared to 60 kD matrix. 150 μ L of 80 kD matrix overfilled an 8mm dermal punch. 200 μ L of 80 kD matrix was successfully delivered by intra-dermal injection although substantial force was required to complete the injection.

10 **Example 29**

Studies were performed to acquire initial rheological data of the CD-PEG₃₄₀₀ matrix (100 mg/ml) (Example 3, method II) before and after crosslinking with di-Adamantane-PEG (36.5 mg/ml) (Example 9, method II). These data were compared to collagen matrix at 2.4 mg/ml, one of the standard formulations used in preclinical
15 model development.

Results:

The first series of experiments were performed with CD-PEG₃₄₀₀ polymer at 100 mg/ml without cross linker. Frequency sweeps at various constant strains were performed.

20 Figure 7 shows a frequency sweep at 37 °C. G'' is greater than G' , resulting in a $\tan\delta$ of approximately 3.2. As expected, this polymer solution exhibits mostly viscous behavior. This is confirmed by the slope of G' as a function of frequency. For purely viscous fluids, a theoretical slope of 2 is expected whereas for purely elastic fluids, a slope of 0 is expected over a certain frequency range. On a structural
25 level, the interpretation of these results is that the polymer molecules interact with each other by some sort of weak interaction. Energy applied to the material can be stored by the molecules elastically by moving nodes of interaction (rotation, entanglement). A large part of this energy is then dissipated into heat. The measured complex viscosity of this polymer solution was 0.27 Pa s at 10.0 rad/s.

Figure 8 shows the same material at 20 °C. An increase in viscosity to 1.46 Pa s at 10 rad/s was observed. This value is approximately 7-fold higher than the viscosity at 37 °C.

Figure 9 shows a frequency sweep for the CD-PEG₃₄₀₀ polymer crosslinked with 36.5 mg/ml of di-Adamantane-PEG. Addition of the cross linker increased the viscosity of the matrix over 100 fold to approximately 33.1 Pa s. At the same time, $\tan \delta$ decreased approximately 3-fold to a value of 1.2 and the slope of G' decreased to 0.58. These results are consistent with an increase in elastic behavior. Structurally, the movement of the polymer within the material is constrained and energy applied can be stored in a more limited way between network points. This behavior is also confirmed by the observation that the crosslinked matrix has a tendency to draw long strings when an immersed object is pulled away from the surface. Over all, viscous forces still are dominant ($\tan \delta > 1$) (see Figure 11).

Figure 10 shows the crosslinked polymer at 20 °C. Viscosity increased further to approximately 50 Pa s while all the other characteristics remained similar.

As a comparison, Figure 11 shows a frequency sweep for the collagen matrix at 2.4 mg/ml. The collagen matrix in its set state (i.e., at 37 °C) exhibits a typical gel behavior, with $\tan \delta$ at a low value of 0.14, a slope of G' of 0.07. Structurally, this is an indication of a permanent and orderly arranged network. Applied energy can only be stored to limited extent between network nodes and is returned to a large extent. The complex viscosity of this material was 12.8 Pa s.

Example 30

In vitro biocompatibility experiment

Methods:

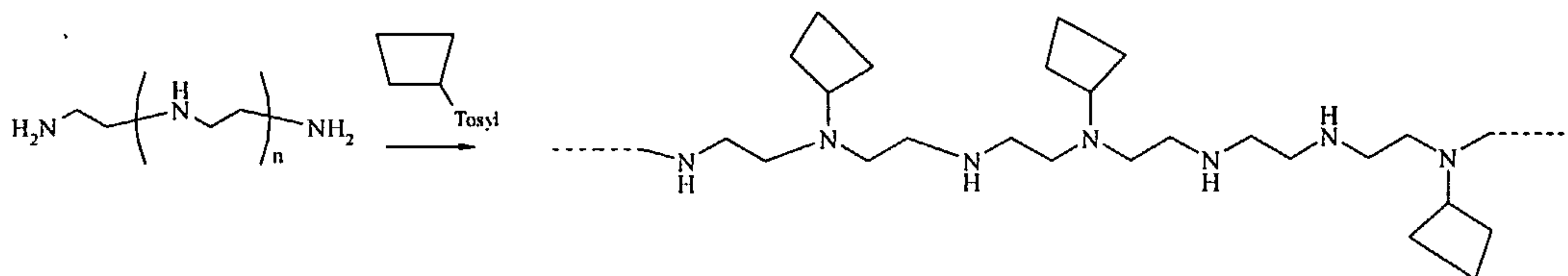
A matrix was prepared using 58 kD cyclodextrin (CD) polymer prepared according to Example 3, method II, and crosslinking agent from Example 9, method II. Upon formulation of the matrix, either pEGFP DNA or GFCB virus was mixed together with the matrix. A low and a high dose of DNA or virus were both

formulated. The various treatment groups are listed in Table 2. Final concentration of 58 kD cyclodextrin matrix was 100 mg/mL for all groups. Approximately 100 μ L of each respective reagent was pipetted into a 48-well flat bottom plate. Each group was tested in duplicate. The 48-well plate containing the test formulations was

5 allowed to set at room temperature for approximately 30 minutes. 2.5×10^4 CCD-1074sk cells (human skin fibroblast) were placed on top of the cross-linked matrix formulations in a volume of 200 μ L of DMEM media containing 10% Fetal Bovine Serum (FBS). The CCD-1074sk cell line was approximately 70% confluent at the time of cell counting with cell viability greater than 95% via Trypan Blue staining.

10 Each well, containing groups 1-8, was examined daily under an inverted microscope for cell viability and for GFP fluorescence signal. 200 μ L of fresh media was added (not replaced) to each of the wells on days 4 and 8 after the start of the experiment. The plate was incubated at 37 °C with 5% CO₂.

Synthesis of CD-IPEI



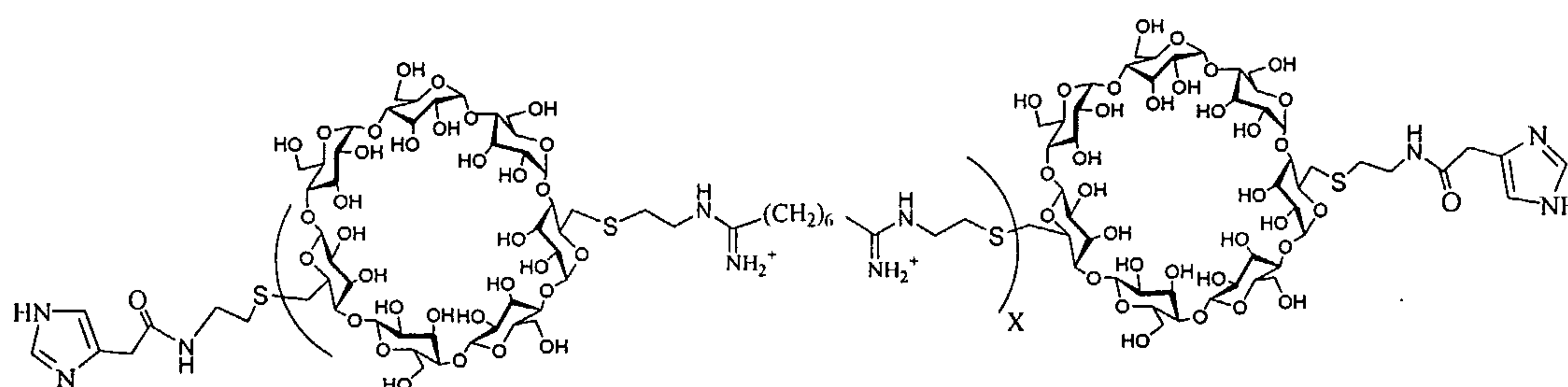
15

Linear PEI_{25,000} (500 mg, Polysciences, Inc.) and 6-Monotosyl- β -Cyclodextrin (3.868 g, Cyclodextrin Technologies Development, Inc.) were dissolved in 36 mL of DMSO. The resulting mixture was stirred at 70°C for 6 days.

20 The solution turned slightly yellow. The solution was then transferred to a Spectra/Por MWCO 10,000 membrane and dialyzed against water for 6 days. Water was then removed by lyophilization to afford a slightly colored solid. Cyclodextrin/PEI ratio was calculated based on the proton integration of ¹H NMR (Varian 300 MHz, D₂O) δ 5.08 ppm (s br., C₁H of CD), 3.3-4.1 ppm (m br. C₂H-C₆H of CD), 2.5-3.2 ppm (m br. CH₂ of PEI).

25

β Cyclodextrin Polymers (CDP-Imidazole).



β CDP was synthesized according to previously described procedures

(Gonzalez, H., Hwang, S. & Davis, M. (1999) *Bioconjugate Chem.* 10, 1068-74).

- 5 Imidazole was conjugated to the β CDP polymer by amidation of the primary amines at the end of the polymer with 4-imidazoleacetic acid (Aldrich, St. Louis, MO) (Sehgal, D. & Vijay, I. (1994) *Anal Biochem.* 218, 87-91). In a typical experiment, 200 mg (33.3 μ mol) of β CDP were dissolved in 800 μ L of 25 mM MES (pH 6.5) buffer to which was added 4-imidazoleacetic acid, sodium salt hydrate (49.3 mg,
- 10 0.333 mmol). This solution was used to dissolve 1-ethyl-3-(3-dimethylaminopropyl)carbodiimide (EDC) (0.128 g, 0.666 mmol). Then, N-hydroxysuccinimide (NHS) (3.83 mg, 33.3 μ mol) dissolved in 200 μ L of 25 mM MES (pH 6.5) buffer was added immediately to the polymer solution. The resulting solution was stirred for 24 h at room temperature and then dialyzed against water
- 15 using a Spectra Por membrane MWCO 1000. The solution was lyophilized to dryness. The imidazole content was determined by the TNBS assay (Hermanson, G. T. (1996) *Bioconjugate Techniques*, pp. 132, Academic Press, Rockford, IL), followed by UV measurements to quantify the amount of unreacted polymer end groups. The imidazole conjugation was 73%.

20 Table 2: Treatment Groups/Well (48-well Flat Bottom Plate)

Group #	Treatment
1	0.25 mg/mL pEGFP + CDP-Imidazole in 58kD Cyclodextrin
2	0.025 mg/mL pEGFP + CDP-Imidazole in 58 kD Cyclodextrin
3	0.25 mg/mL pEGFP + CD-1PEI in 58 kD Cyclodextrin
4	0.025 mg/mL pEGFP + CD-1PEI in 58 kD Cyclodextrin

5	1 x 10 ¹⁰ P/mL GFCB in 58 kD Cyclodextrin
6	1 x 10 ⁹ P/mL GFCB in 58 kD Cyclodextrin
7	Empty Control (Cells Alone)
8	58 kD Cyclodextrin Matrix Alone Control

Results:

Day 1: Groups 1-4 started dying. They were starting to lift off the plate. CCD-1074sk cells were “rounded up” morphologically and floating. Groups 5-8 looked healthy. The cells were attached to the plate and “stretched out” morphologically (typical state of fibroblasts); however, none of the groups had GFP expression at this time. See Figure 12.

Day 2: Groups 5-8 looked healthy. CCD-1074sk cells were attached to the plate and “stretched out”. Groups 5-6 (GFCB groups) were positive for GFP expression. The higher dose of GFCB (Group 5) had more GFP expression than the lower dose of GFCB (Group 6). Groups 1, 3, and 4 looked to be completely dead at this time; however, a couple cells had survived in group 2 (0.025 mg/mL pEGFP + CDP-Imidazole in 58 kD Cyclodextrin). There was no detectable GFP expression in groups 1-4.

Day 4: CCD-1074sk cells in groups 1-4 appeared to be dead. Cells were floating. GFP expression was not detectable in any of these groups. Groups 5-8 were healthy. Groups 5-6 were positive to GFP expression, and expression appeared to be even brighter than the day 2.

Day 5: CCD-1074sk cells in group 1-4 were dead and no GFP expression was seen. Groups 5-8 were healthy. Groups 5-6 were positive for GFP expression and once again the expression level appeared to be brighter than the day before.

Day 6: CCD-1074sk cells in groups 1-4 were dead and no GFP expression was seen. Cells were no longer monitored. Groups 5-8 were healthy. Groups 5-6 were still expressing GFP and the expressions level appeared to still be brighter than the day before.

Day 8: CCD-1074sk cells in groups 5-8 still looked healthy. Morphologically, they did not look any different from day 6. They were still expressing GFP and appeared to be at the brightest observed intensity.

Day 12: CCD-1074sk cells in groups 5-8 were healthy. Cell count seemed to be slightly more numerous than day 8; however, GFP expression appeared to be decreasing.

Day 13: CCD-1074sk cells in groups 5-8 appeared healthy, but GFP expression was starting to decrease.

Example 29

10 Methods:

The components for Matrix A and Matrix B were formulated following the written protocol from Insert Therapeutics, Inc. Matrix A was 100 mg/mL of β -Cyclodextrin-PEG₃₄₀₀ polymer (Example 3, method II) in PBS at pH of 7.2 with 4.4 mg/mL of di-Adamantane compound crosslinker (Example 9, method II). The two components were aliquoted and kept separate until used. Matrix B was 100 mg/mL of β -Cyclodextrin-PEG₃₄₀₀ polymer in PBS at a pH of 7.2 with 36.5 mg/mL of di-Adamantane PEG₃₄₀₀ compound crosslinker. The components were aliquoted and kept separate.

Three different methods of delivery were tested:

20 1) *Delivery of Matrix A into a Wound Site Using a Surgical Dressing and Delivery of Matrix B into a Wound Site Prior to Covering with a Surgical Dressing:*

An ICR mouse was anesthetized with ketamine and xylazine. The dorsal region was shaved and two 8 mm dermal punches were made. 50 μ L of Matrix A (final adjusted volume) was mixed containing a small amount of dye and then placed onto a small square piece of OpSite dressing. The matrix was allowed to gel for about 2 minutes. During this time, the left wound punch on the mouse was prepared with Mastisol dressing adhesive. The OpSite dressing containing the mixed Matrix A was then flipped over ("sticky" side down) and placed over the left wound site. The right wound punch was prepared with Mastisol adhesive dressing. Matrix B

containing a small amount of dye was also made up at a final adjusted volume of 50 μL and placed directly onto the right wound site. This was allowed to gel for about 2 minutes then covered with the OpSite dressing. This animal was allowed to recover from surgery and was sacrificed 4 days later.

5 2) *Delivery of Matrix A with Pre-Mixing and Matrix B without Pre-Mixing into a Wound Site Through a Previously Applied Surgical Dressing:*

An ICR mouse was anesthetized with ketamine and xylazine. The dorsal region was shaved and two 8 mm dermal punches were made. Two wound sites were prepared with Mastisol adhesive and 1 single sheet of OpSite dressing was placed over the wounds. Matrix A was prepared for a 50 μL total injection volume containing a small amount of dye. The matrix was drawn up directly into a 1 cc syringe and a 23G needle was placed on the syringe. Excess matrix was expelled from the syringe until approximately 50 μL remained. This material was then injected through the OpSite dressing onto the left wound bed. For the right side wound, Matrix B was prepared for ~ 100 μL total injection volume. A 1 cc syringe containing a 23G needle was used to draw up approximately 82 μL of Matrix B. A small air pocket was then drawn into the syringe. Approximately 18 μL of the accompanying crosslinker was then drawn into the same syringe needle. Another small air pocket was then drawn into the syringe. Finally, a small amount ($\sim 2-4$ μL) of dye was drawn into the syringe. A 27G needle was placed at one end of the right wound site through the dressing to vent air from the covered wound site. The syringe with a 23G needle containing the separated components of Matrix B was placed through the dressing (without pre-mixing of the components) and the materials were injected into the wound site. The 27G needle provided venting of the small air pockets in the syringe. The animal was allowed to recover after surgery and was sacrificed 4 days later.

3) *Injection of Matrix A and B into PVA Sponges Using Various Gauge Needles:*

An HSD rat was anesthetized with ketamine and xylazine and PVA sponges were subcutaneously implanted onto the ventral side of the rat. Incisions were closed with wound clips and the animal was allowed to recover for 4 days. Matrix A

was formulated at an adjusted injection volume of ~ 200 μ L with dye (~ 2-4 μ L). The matrix mixture was drawn into a 1 cc syringe through a 22G needle and mixed in the syringe. Attempts were made to remove excess air bubbles. The mixed matrix was injected into the center of a PVA sponge on a sacrificed animal. After a
5 few minutes, the wound site was opened and the sponge area was examined.

Matrix B was prepared for ~ 200 μ L injection. The matrix contained a small amount of dye and was drawn into a 1 cc syringe using a 22G needle, which was removed and replaced with a shorter 23G needle for injection. The materials were mixed in the syringe and an attempt to remove excess air bubbles was made. Matrix
10 was injected into the center of a PVA sponge, allowed to sit for a few minutes, and then the animal was opened for examination of the injected sponge.

Results:

1) Delivery of Matrix A into a Wound Site Using a Surgical Dressing and Delivery of Matrix B into a Wound Site Prior to Covering with a Surgical Dressing:

15 50 μ L of Matrix A (final adjusted volume) was mixed with a small amount of dye, placed onto a small square piece of OpSite dressing, allowed to gel for a short period of time (~ 2 minutes), and then flipped over ("sticky" side down) on the left wound site. Upon sacrifice of the animal 4 days after surgery, the wound appeared to be dry and the animal was observed to have tolerated Matrix A without
20 difficulties. Matrix appeared to stay in its original position at the time of delivery, i.e., on top of the wound site including some of the surrounding unwounded tissue. The matrix that remained in the wound site was superficial and less abundant than the day of surgery. No gross appearance of inflammation was seen at the wound site. See Figures 12A-12B.

25 Matrix B containing a small amount of dye was also made up at a final adjusted volume of 50 μ L and placed directly onto the right wound site and then covered with OpSite dressing. When the animal was sacrificed 4 days later, the wound appeared to be dry and the animal seemed to have tolerated Matrix B well. No inflammation or any other adverse effects were grossly seen around the wound

site. The matrix did not disperse onto surrounding tissue after surgery, but rather stayed in the original wound site. The matrix that remained in the wound site at the time of sacrifice was superficial and less abundant than at the day of surgery. See Figures 12A-12B.

5 2) *Delivery of Matrix A with Pre-Mixing and Matrix B without Pre-Mixing into a Wound Site Through a Previously Applied Surgical Dressing:*

50 μ L of Matrix A (final adjusted volume) was mixed with a small amount of dye and then injected directly under the OpSite dressing and on the left wound site. The matrix remained localized in the wound site and did not disperse to the
10 surrounding unwounded tissue. Due to air bubbles in the syringe, it was not possible to make precise measurements of the dosing volume. Upon sacrifice of the animal 4 days after surgery, the wound appeared to be dry and the animal tolerated Matrix A without any observable adverse effects. The matrix stayed in its original position at delivery, i.e., at the wound site including some surrounding unwounded tissue. The
15 matrix did not disperse onto other surrounding tissue after the surgery; however, the matrix was only on the surface of the wound and less abundant than at the time of surgery. Upon gross examination, no inflammation was seen at the wound site. See Figures 13A-13B.

100 μ L final volume of Matrix B containing a small amount of dye was
20 drawn into a syringe. The various components of the matrix (polymer, crosslinker, and dye) were drawn individually into the syringe with air pockets to separate the individual components. A venting needle to eliminate the air pockets in the syringe was placed in one end of the wound through the dressing and the separated components of Matrix B were injected directly onto the right wound site through the
25 OpSite dressing without any prior mixing. This method required the least amount of pressure to successfully inject the matrix into the wound site, and the venting needle worked to eliminate air pockets under the skin. Once all the components of Matrix B were delivered into the wound site, the matrix gelled quickly by visual elimination and touch, and no matrix leaked out of the dressing. The matrix remained localized
30 to the wound bed and did not grossly spread to surrounding tissues. When the

animal was sacrificed 4 days later, the wound appeared to be dry and the animal seemed to have tolerated Matrix B without gross adverse effects. No inflammation or any other adverse effects were seen around the wound site, and the matrix appeared to stay in the local wound area. The matrix was localized to the surface of the wound and at lower amounts than at the original time of injection. See Figures 13A-13B.

3) Injection of Matrix A and B into PVA Sponges Using Various Gauge Needles:

Matrix A was prepared with a small amount of dye and drawn into a 1 cc syringe through a 22G needle. Approximately 200 μ L of the matrix was injected into a PVA sponge, allowed to sit for a few minutes, and then the animal was opened for examination. Upon examination of the sponge, the matrix appeared to remain localized and had minimal dispersion to the surrounding areas.

Matrix B was prepared, mixed with a small amount of dye, and drawn into a 1 cc syringe with a 22G needle. The 22G needle (1 1/2 inches) was replaced with a shorter 23G needle (1 inch). Approximately 200 μ L of the matrix was injected into a PVA sponge, allowed to sit for a few minutes, and then the animal was opened for examination. Upon further examination of the sponge, the matrix appeared to remain localized and had minimal dispersion to the surrounding areas.

Conclusion:

Matrix A and Matrix B both gelled extremely quickly and were very viscous and thick. Even though it is possible to inject the matrices subcutaneously and into PVA sponges, the easiest method of delivery was to draw the various components of the matrix separately (separated by a small pocket of air) into a syringe and then inject directly through a covered dermal punch using a 23G needle. In this method, a second smaller gauge needle can assist in venting excess air from under the wound dressing.

Example 30

Platelet derived growth factor B (PDGF-B) has been shown to stimulate fibroblast proliferation and the synthesis of extracellular matrix. PDGF-B expression was compared by RT-PCR for cyclodextrin and collagen matrices in the rat PVA sponge model.

Animal # 200 μ L Total Injection Volume/Sponge	Grp #	Sponge Injection Contents
6 (N = 6 Sponges/Group)	1: 2: 3: 4: 5: 6:	Collagen alone 58 kD Cyclodextrin(CD)-Adamantane Matrix alone 2×10^{10} PN PGCB in Collagen 2×10^{10} PN PGCB in CD-Adamantane Matrix 50 μ g pCTK-PD (plasmid DNA encoding PDGF-B) + L-PEI in CD-Adamantane Matrix 50 μ g pCTK-PD + CD _{Imidazole} in CD-Adamantane Matrix

Methods

Six small incisions (0.5 cm) were performed and polyvinyl alcohol (PVA, *M-PACT®*) sponges were subcutaneously implanted on the ventral side of male Harlan Sprague-Dawley rats. Four days after implantation, test and control materials were diluted with vPBS and liquid collagen (*Cohesion Technologies®*) or 58 kD Cyclodextrin (CD)-Adamantane matrix as described above and injected into PVA sponges. Final collagen formulation was 1.8 mg/mL, pHed with NaOH, and brought up to volume with vPBS. Final 58 kD Cyclodextrin (CD)-Adamantane matrix formulation was 100 mg/mL. 200 μ L total volume of test reagent was delivered to each sponge. Animals were sacrificed and sponges were removed 2 days after injections. Sponges were cut into three pieces and the majority of the sponge (~ 70-80%) was frozen in liquid nitrogen and stored at -80 °C for QPCR and QRT-PCR analysis. A small portion of the sponge was fixed in 4% PFA at 4 °C for 18 hours,

paraffin embedded, and sectioned (5 μ m). Sections were stained using Masson's Trichrome (cells = black, vasculature = red, and collagen = blue) and Hematoxylin-Eosin methods. Tissue sections were analyzed microscopically for gross histology by two separate investigators.

5 Results:

Implanted PVA sponges were treated with either collagen, cyclodextrin matrix (CD), 2×10^{10} PN of PGCB in Collagen, 2×10^{10} PN of PGCB in CD, 50 μ g of pCTK-PD + L-PEI in CD, or 50 μ g pCTK-PD + CD_{Imidazole} in CD. Sponges were removed 48 hours after treatment and assayed for human PDGF-B RNA and viral
10 DNA by QRT-PCR and QPCR methods, respectively. A portion of each sponge was also fixed, embedded, sectioned, and stained using Masson's Trichrome for gross morphological examination.

QRT-PCR (quantitative RT-PCR) analysis for human PDGF-B RNA expression showed that sponges treated with 2×10^{10} PN of PGCB in CD had the
15 highest average RNA content of 7.0×10^8 MEQ of PDGF-B/assayed sponge (Figure 14). Sponges treated with 2×10^{10} PN of PGCB in Collagen had similar average levels of PDGF-B RNA at 3.2×10^8 MEQ of PDGF-B/assayed sponge. Sponges treated with 50 μ g of pCTK-PD + L-PEI in CD and 50 μ g pCTK-PD CD_{Imidazole} in CD had PDGF-B RNA levels of 6.8×10^5 and 9.1×10^4 MEQ of PDGF-B/assayed
20 sponge, respectively. Finally, sponges treated with either Collagen or Cyclodextrin showed no detectable levels of PDGF-B RNA (Figure 14, Table 3). A Student's t-test analysis showed that all sponge treatment groups were statistically different ($p \leq 0.05$) except for the sponge comparisons between 2×10^{10} PN of PGCB in collagen and 2×10^{10} PN of PGCB in CD (Table 4). GAPDH QRT-PCR control assays were
25 also performed to monitor RNA quality and total RNA per sample. The results showed a consistent amount of RNA ranging from 1.9×10^7 to 6.9×10^7 MEQ of GAPDH/assayed sponge for all treatment groups (Figure 15).

Table 3: QRT-PCR Results for hPDGF-B RNA Detection.

Group	Count (n)	Mean	Std. Dev.	Std. Err.
Collagen	6	BQL	•	•
58 kD CD	5	BQL	•	•
2 x 10 ¹⁰ PN PGCB in Collagen	6	3.2E+8	2.0E8	8.2E+7
2 x 10 ¹⁰ PN PGCB in CD	6	7.0E+8	4.1E+8	1.7E+8
50 µg pCTK-PD + L-PEI in CD	6	6.9E+5	2.9E+5	1.2E+5
50 µg pCTK-PD + CD _{Imidazole} in CD	6	9.1E+4	1.7E+5	7.1E+4

BQL = Below Quantitation Levels ($< 2 \times 10^3$ MEQ of PDGF-B/Assayed Sponge)

MEQ = Molecular Equivalent is an arbitrarily assigned number based on the dilution factor of a positive control.

5

Table 4: Statistical Analysis of hPDGF-B RNA between Treatment Groups.

Unpaired Comparison of Treatment Groups	p-Value
2 x 10 ¹⁰ PN PGCB in Collagen vs. 2 x 10 ¹⁰ PN PGCB in CD	0.0699
2 x 10 ¹⁰ PN PGCB in Collagen vs. 50 µg pCTK-PD + L-PEI in CD	0.0030
2 x 10 ¹⁰ PN PGCB in Collagen vs. 50 µg pCTK-PD + CD _{Imidazole} in CD	0.0030
2 x 10 ¹⁰ PN PGCB in CD vs. 50 µg pCTK-PD + L-PEI in CD	0.0020
2 x 10 ¹⁰ PN PGCB in CD vs. 50 µg pCTK-PD + CD _{Imidazole} in CD	0.0020
50 µg pCTK-PD + L-PEI in CD vs. 50 µg pCTK-PD + CD _{Imidazole} in CD	0.0014

Note: Statistical analyses could not be performed for collagen and 58 kD CD treatment groups.

10 QPCR (quantitative PCR) analysis for human PDGF-B DNA showed that sponges treated with 50 µg of pCTK-PD + L-PEI in CD and 50 µg pCTK-PD +

CD_{Imidazole} in CD had the highest average levels at 2.4×10^{12} and 1.7×10^{12} MEQ of PDGF-B/assayed sponge, respectively (Figure 16, Table 5). Sponges treated with 2×10^{10} PN of PGCB in Collagen and 2×10^{10} PN of PGCB in CD had average human PDGF-B DNA levels of 4.5×10^{10} and 4.1×10^{10} MEQ of PDGF-B/assayed sponge, respectively. However, sponges treated with collagen or cyclodextrin also had positive PDGF-B DNA levels at 9.8×10^8 and 1.3×10^8 MEQ of PDGF-B/assayed sponge, respectively. A Student's t-test analysis showed that all groups were statistically different ($p \leq 0.05$) except for sponge comparisons between collagen and cyclodextrin and between 2×10^{10} PN of PGCB in collagen and 2×10^{10} PN of PGCB in CD treatment groups (Table 6). Mouse GAPDH quantification was performed to ensure the quality of DNA and equal amount of DNA input, and the results ranged from 9.4×10^8 to 2.8×10^9 MEQ of GAPDH/assayed sponge (Figure 17).

Table 5: PCR Results for Viral PDGF-B Detection within Sponges

Group	Count (n)	Mean	Std. Dev.	Std. Err.
Collagen	6	9.8E+8	1.5E+9	6.1E+8
58 kD CD	5	1.3E+8	2.1E+8	9.2E+7
2×10^{10} PN PGCB in Collagen	6	4.5E+10	3.9E+10	1.6E+10
2×10^{10} PN PGCB in CD	6	4.1E+10	2.3E+10	9.2E+9
50 μ g pCTK-PD + L-PEI in CD	6	2.4E+12	1.1E+11	4.6E+10
50 μ g pCTK-PD + CD _{Imidazole} in CD	6	1.7E+12	4.1E+11	1.7E+11

15

Table 6: Statistical Analysis of human PDGF-B DNA Content within Sponges

Unpaired Comparison of Treatment Groups	p-Value
Collagen vs. 58 kD CD	0.2382
Collagen vs. 2×10^{10} PN PGCB in Collagen	0.0207
Collagen vs. 2×10^{10} PN PGCB in CD	0.0015
Collagen vs. 50 μ g pCTK-PD + L-PEI in CD	< 0.0001
Collagen vs. 50 μ g pCTK-PD + CD _{Imidazole} in CD	< 0.0001
58 kD CD vs. 2×10^{10} PN PGCB in Collagen	0.0321
58 kD CD vs. 2×10^{10} PN PGCB in CD	0.0030
58 kD CD vs. 50 μ g pCTK-PD + L-PEI in CD	< 0.0001
58 kD CD vs. 50 μ g pCTK-PD + CD _{Imidazole} in CD	< 0.0001
2×10^{10} PN PGCB in Collagen vs. 2×10^{10} PN PGCB in CD	0.8197
2×10^{10} PN PGCB in Collagen vs. 50 μ g pCTK-PD + L-PEI in CD	< 0.0001
2×10^{10} PN PGCB in Collagen vs. 50 μ g pCTK-PD + CD _{Imidazole} in CD	< 0.0001
2×10^{10} PN PGCB in CD vs. 50 μ g pCTK-PD + L-PEI in CD	< 0.0001
2×10^{10} PN PGCB in CD vs. 50 μ g pCTK-PD + CD _{Imidazole} in CD	< 0.0001
50 μ g pCTK-PD + L-PEI in CD vs. 50 μ g pCTK-PD + CD _{Imidazole} in CD	0.0018

QPCR results showed significant levels of PDGF-B DNA detected in collagen and cyclodextrin control sponges. The source of the contribution for this observation has not been completely determined; however, hexon QPCR results, which will only detect hexon sequence contained in adenovirus, indicated that DNA detected in control sponges derived from PCTK-PD plasmid (Figure 18). Since PDGF-B RNA was not detected in control sponges, this suggests that contamination most likely occurred at or after the time of sponge harvest.

Table 7: Summary PVA Sponge Morphological Analysis.

Group	Capsule Size	Immune Response	Granulation Tissue	Collagen Deposition	Vasculature
Collagen	Thin	Minimal	Minimal	Minimal	Minimal
58 kD CD	Thin to Moderate	Light to Moderate	Minimal to Light	Minimal	Light to Moderate
2 x 10 ¹⁰ PN PGCB in Collagen	Thick	Moderate	Minimal to Light	Light	Moderate to Heavy
2 x 10 ¹⁰ PN PGCB in CD	Very Thick	Severe	Minimal to Light	Light	Moderate
50 µg pCTK-PD + L-PEI in CD	Thin to Moderate	Light to Moderate	Minimal to Light	Minimal	Light to Moderate
50 µg pCTK-PD + CD _{Imidazole} in CD	Thin to Moderate	Light to Moderate	Minimal to Light	Minimal	Light to Moderate

5 µm, Masson's Trichrome stained paraffin sections were analyzed by two separate observers. Sponge characteristics were qualitatively evaluated by the following criteria: Minimal < Light < Moderate < Heavy < Severe for all categories except Capsule Size. The following criteria were used for evaluation of Capsule Size: Thin < Moderate < Thick < Very Thick.

Morphological analysis of the sponges was performed to evaluate host immune responses. Although this study was designed with gene expression and inflammation as primary endpoints, granulation tissue formation, collagen deposition, and neo-vascularization were also analyzed when present. Upon harvest, sponges treated with 2 x 10¹⁰ PN of PGCB in CD had an observable and elevated

amount of exudate within and surrounding the sponges (Table 7, Figure 19). These sponges were also much larger in size than other groups. Gross histological examination revealed that sponges treated with 2×10^{10} PN of PGCB in CD had a severe immune response characterized by a thick capsule and the presence of cellular
5 infiltrate. Granulation tissue, collagen, and neo-vascularization were also observed. Sponges treated with 2×10^{10} PN of PGCB in collagen also showed granulation tissue formation, collagen deposition, and neo-vascularization; however, the immune response was not as severe as sponges treated with PGCB in CD. Sponges treated with cyclodextrin alone, 50 μ g of pCTK-PD + L-PEI in CD, or 50 μ g pCTK-PD +
10 CD_{Imidazole} in CD all had similar results with minimal amounts of granulation tissue. The overall immune response found in these treatments groups was similar to sponges treated with PGCB in collagen. Finally, sponges treated with the collagen alone were found to have minimal amounts of tissue, collagen, or vasculature as well as a minimal immune response.

15

All of the above-cited references and publications are hereby incorporated by reference.

Those skilled in the art will recognize, or be able to ascertain using no more than routine experimentation, many equivalents to the specific embodiments of the
20 invention described herein. Such equivalents are intended to be encompassed by the following claims.

Claims

1. A polymer composition comprising a linear biocompatible polymer including a plurality of inclusion hosts, and linking molecules, each linking molecule comprising at least two moieties that form inclusion complexes with the inclusion hosts, wherein the linking molecules crosslink the polymer.
2. A polymer composition of claim 1, wherein the inclusion hosts are cyclodextrin moieties.
3. A polymer composition of claim 1, further comprising at least one biologically active compound or a prodrug form thereof.
4. A polymer composition of claim 3, wherein the biologically active compound is a nucleic acid.
5. A polymer composition of claim 4, wherein the nucleic acid is provided in a delivery system selected from a virus, a polymer, and a liposome.
6. A method for transfecting a cell with a nucleic acid, comprising contacting the cell with a polymer composition of claim 4.
7. A polymer composition of claim 3, wherein the compound is a polypeptide or a small organic molecule.
8. A method for administering a biologically active compound to a patient, comprising administering to the patient a polymer composition of claim 3.
9. A polymer composition of claim 3, wherein the compound is a protein or polypeptide.
10. A polymer composition of claim 3, wherein the biologically active compound or prodrug form thereof is provided in a delivery system.

11. A polymer composition of claim 10, wherein the delivery system is selected from microparticles and liposomes.
12. A polymer composition of claim 3, wherein the biologically active compound is covalently attached to a moiety that forms an inclusion complex with the inclusion host.
13. A polymer composition of claim 1, further comprising at least one adjuvant.
14. A polymer composition of claim 3, further comprising an adjuvant that increases the effectiveness of the biologically active agent.
15. A polymer composition comprising a biocompatible, biodegradable polymer including a plurality of inclusion hosts, and linking molecules, each linking molecule comprising at least two moieties that form inclusion complexes with the inclusion hosts, wherein the linking molecules crosslink the polymer.
16. A polymer composition comprising a biocompatible polymer including a plurality of inclusion hosts, and linking molecules, each linking molecule comprising at least three moieties that form inclusion complexes with the inclusion hosts, wherein the linking molecules crosslink the polymer.
17. A polymer composition comprising a biocompatible polymer including a plurality of cyclodextrin moieties, and linking molecules, each linking molecule comprising at least two moieties that form inclusion complexes with the cyclodextrin moieties, wherein each cyclodextrin moiety has no more than two bonds to the polymer backbone, and the linking molecules crosslink the polymer.
18. A therapeutic composition comprising a) a biocompatible polymer including a plurality of inclusion hosts, b) linking molecules, each linking molecule comprising at least two moieties that form inclusion complexes with the inclusion hosts, and c) a therapeutic agent, wherein the linking molecules crosslink the polymer.

19. A method for preparing a crosslinked polymer, comprising combining a linear, biocompatible polymer including inclusion hosts with linking molecules, each linking molecule comprising at least two moieties that form inclusion complexes with the inclusion hosts.
20. A method of claim 19, wherein the inclusion hosts are cyclodextrins.
21. A method of claim 19, wherein the polymer and linking molecules are combined in the presence of a biologically active agent.
22. A method of claim 21, wherein the biologically active agent is covalently linked to a moiety that forms an inclusion complex with the inclusion hosts.
23. A method for preparing a crosslinked polymer, comprising combining a polymer including inclusion guests with linking molecules, each linking molecule comprising at least two inclusion hosts that form inclusion complexes with the inclusion guests.
24. A method of claim 23, wherein the inclusion hosts are cyclodextrin.
25. A method of claim 23, wherein the polymer and linking molecules are combined in the presence of a biologically active agent.
26. A method of treating a disease, comprising administering to a patient an agent suitable for treating the disease in combination with a polymer composition of claim 1.
27. The method of claim 26, wherein the disease is cancer.
28. A method of treating a wound, comprising applying to the wound a polymer composition of claim 1.
29. The method of claim 28, wherein the composition further comprises a therapeutic agent.
30. The method of claim 29, wherein the agent is a nucleic acid encoding PDGF-B.

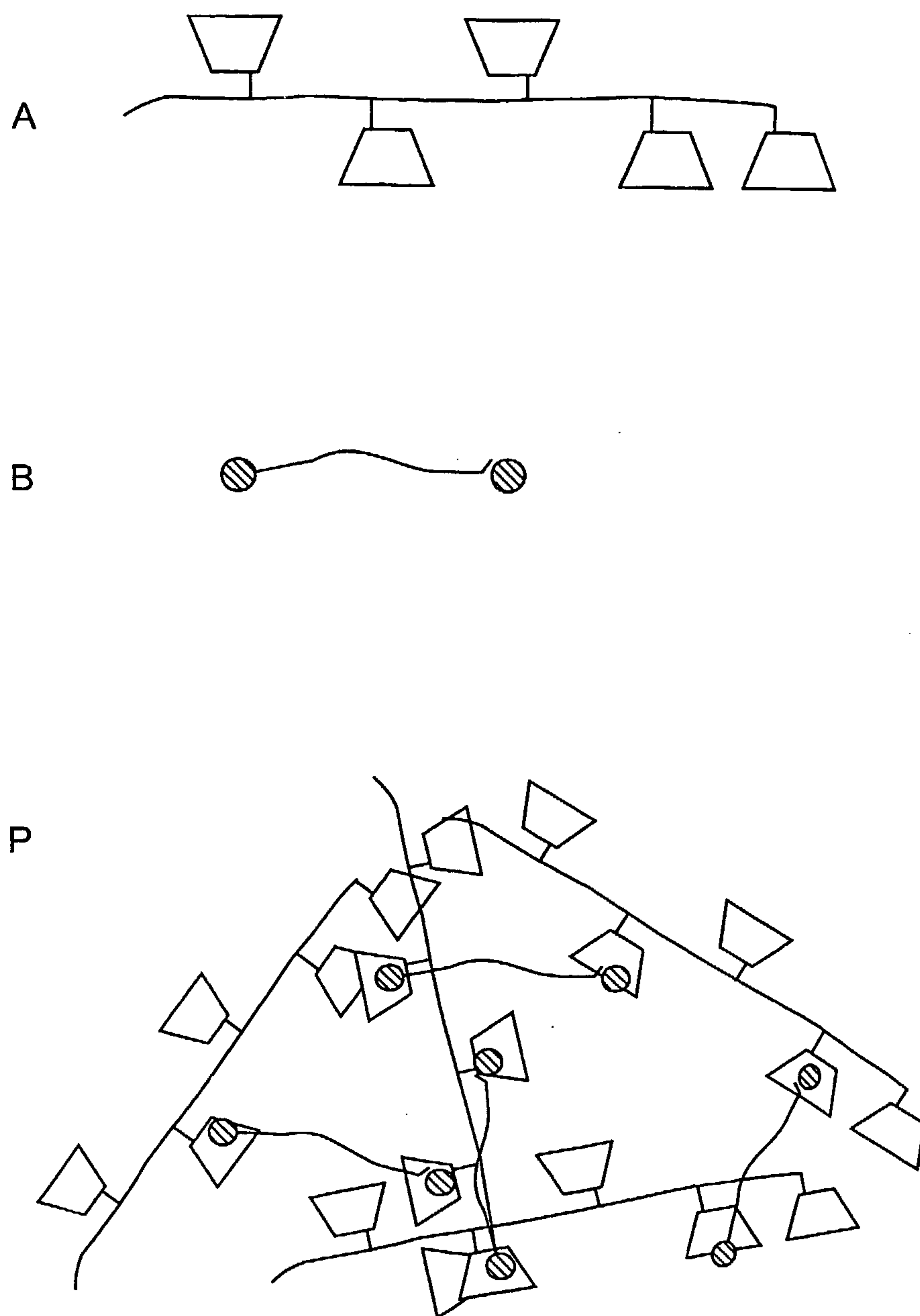


Figure 1

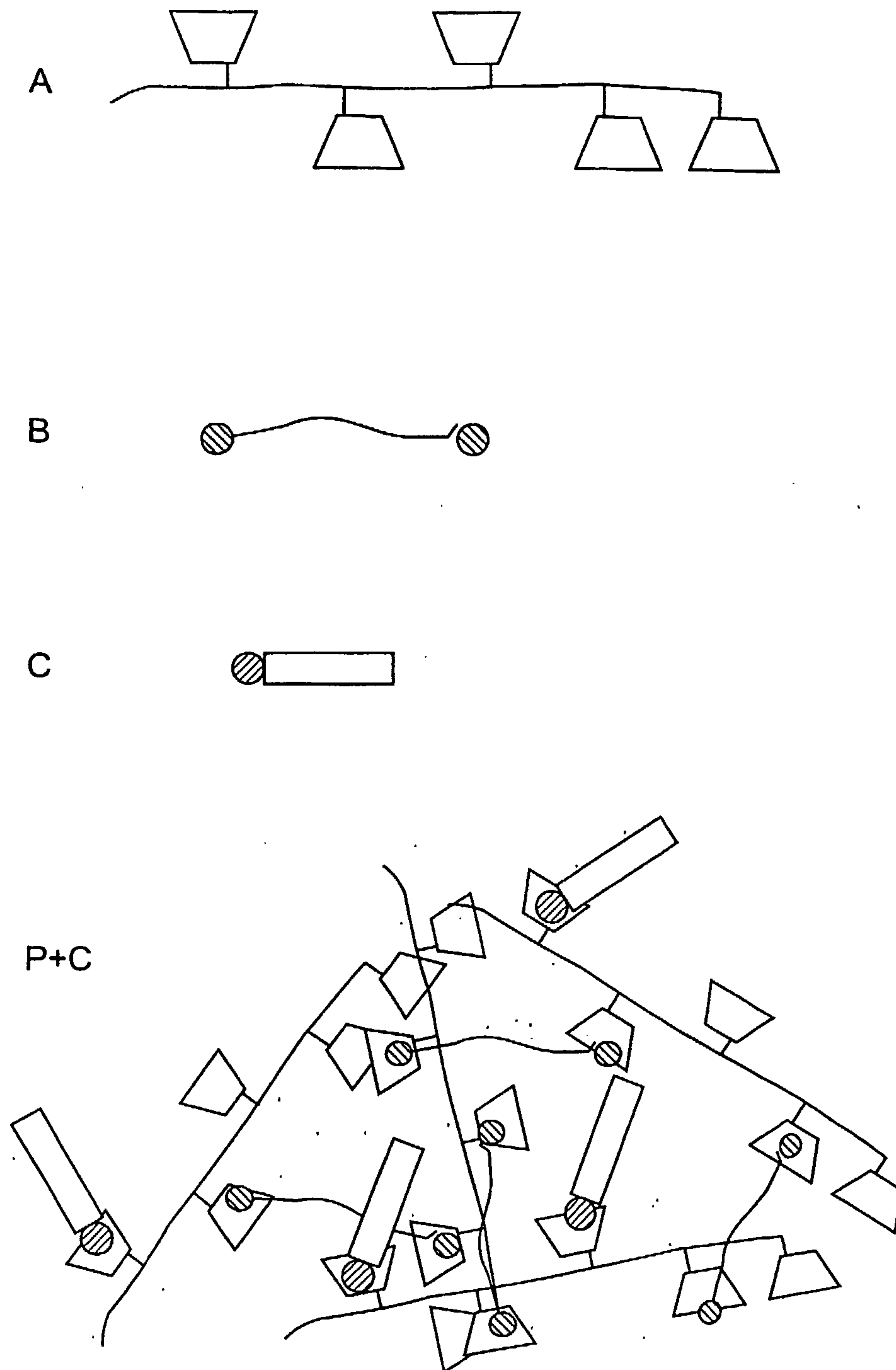


Figure 2

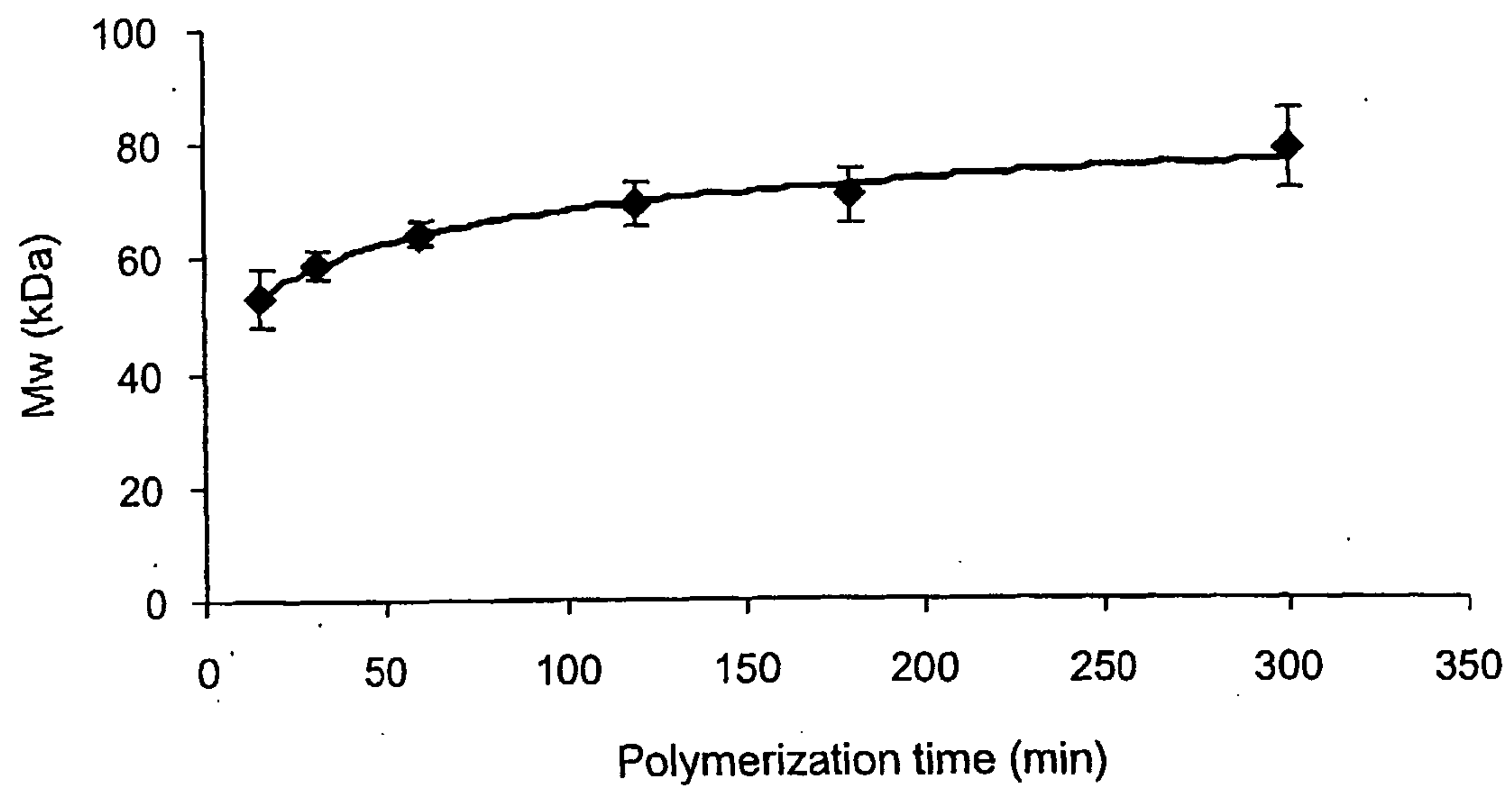


Figure 3

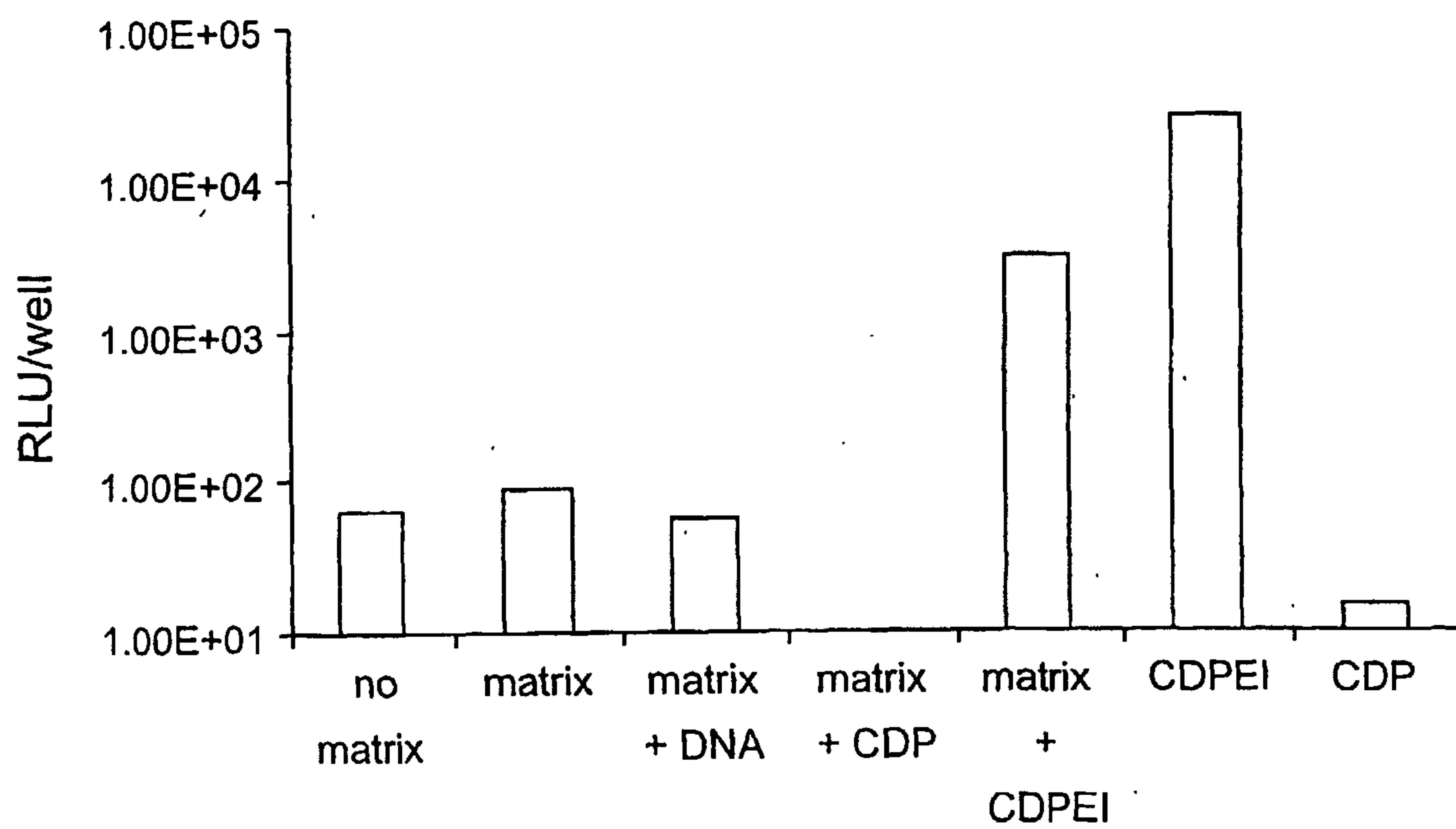
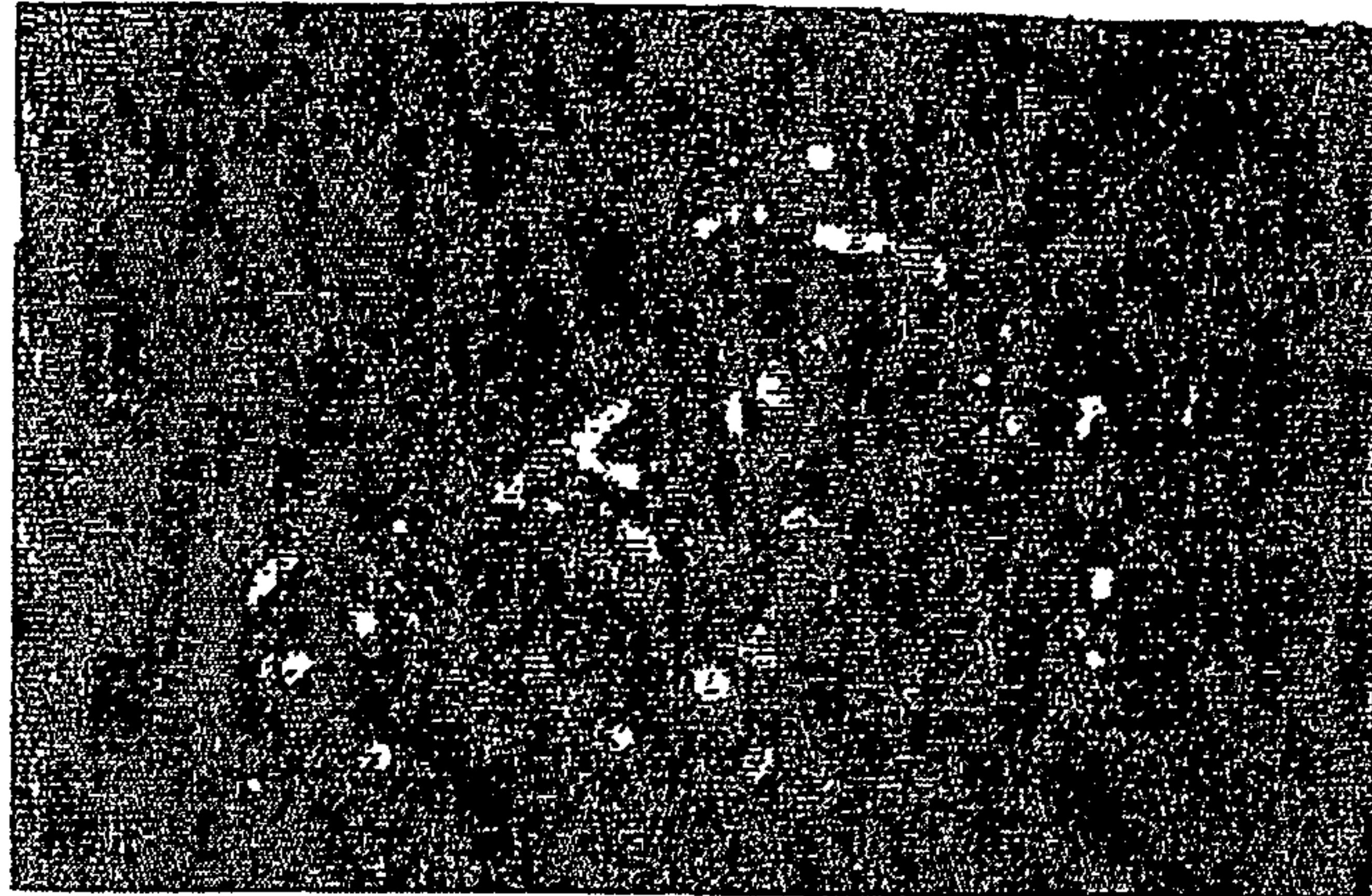
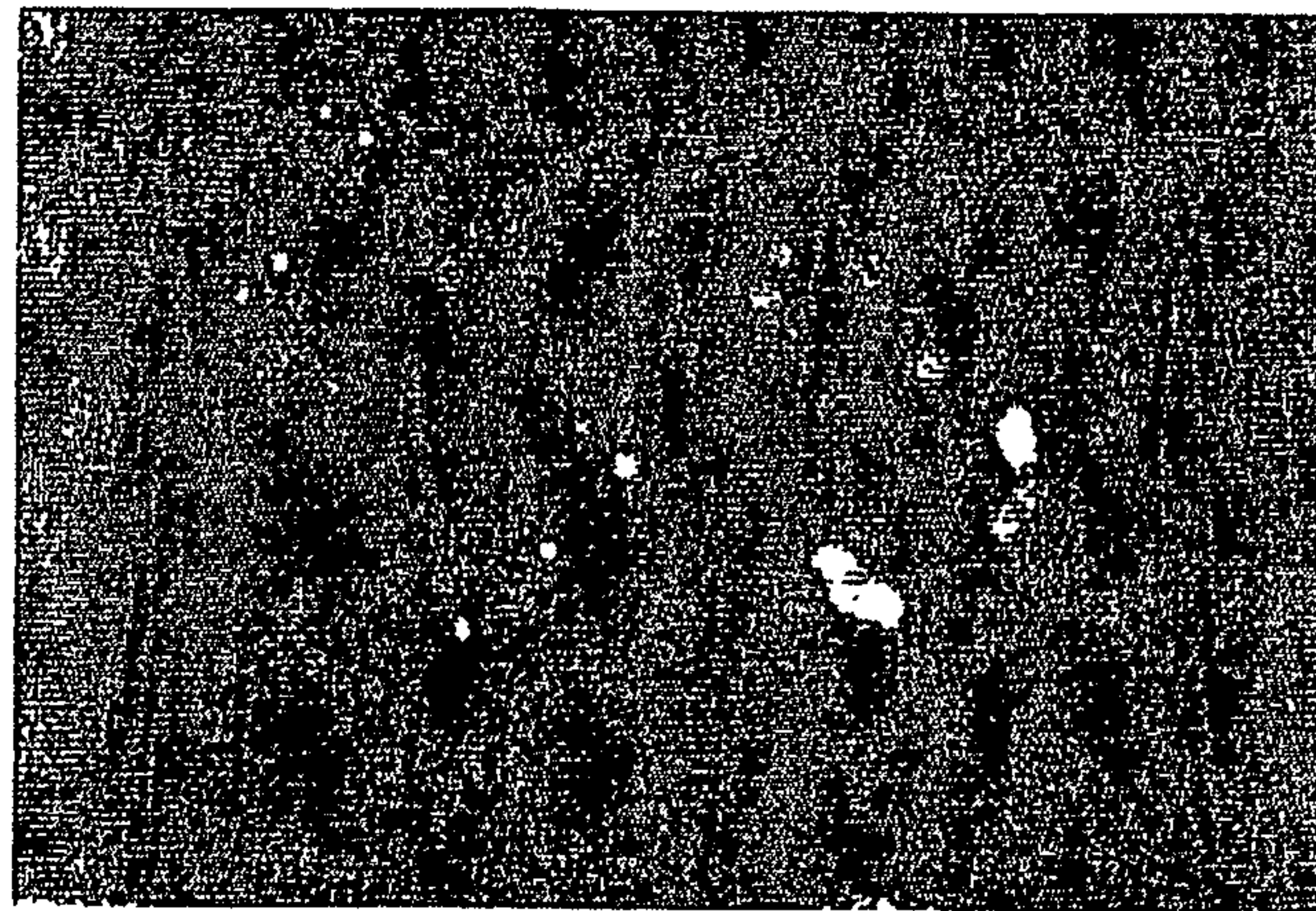


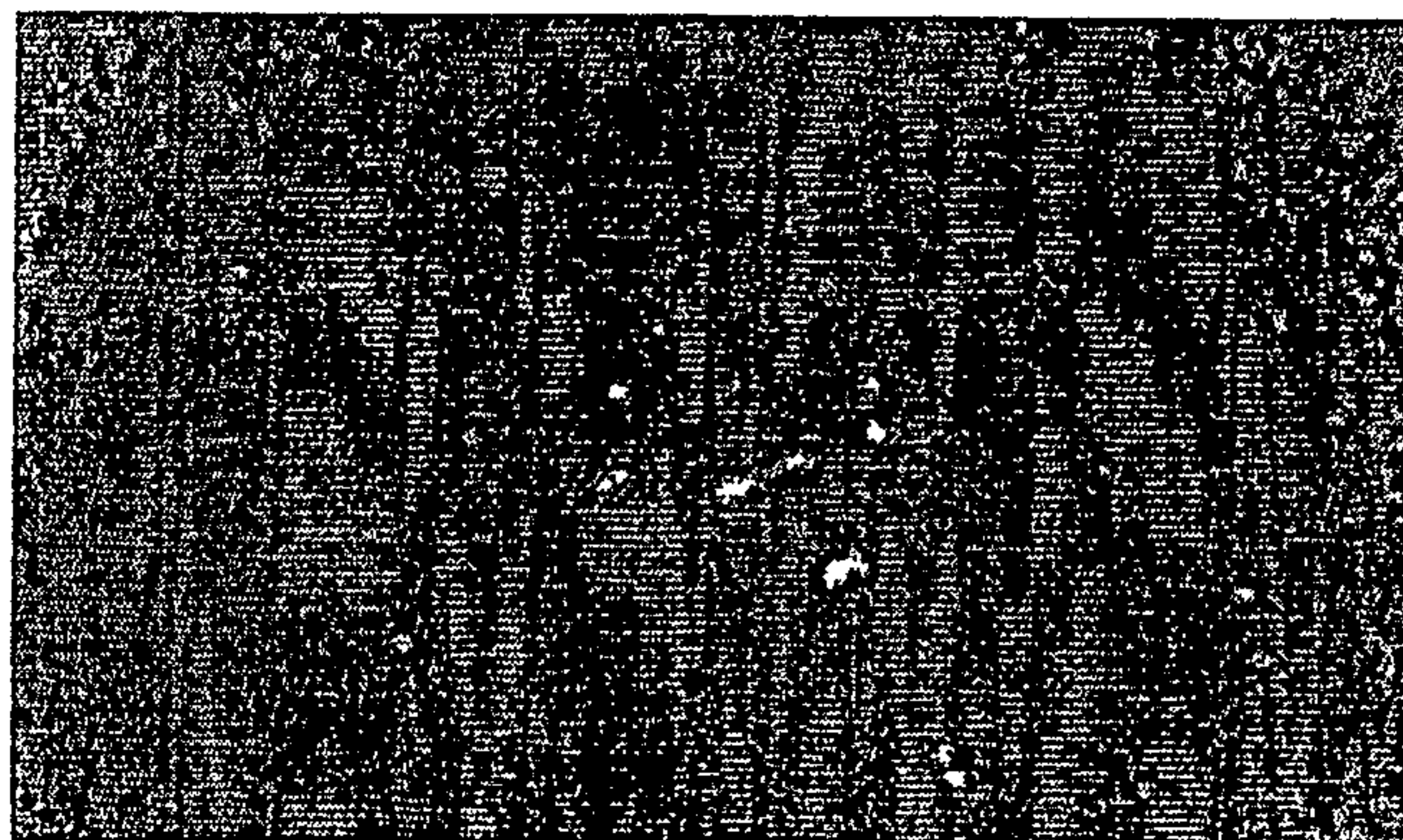
Figure 4



No Matrix



Matrix + PDGF



Matrix

Figure 5

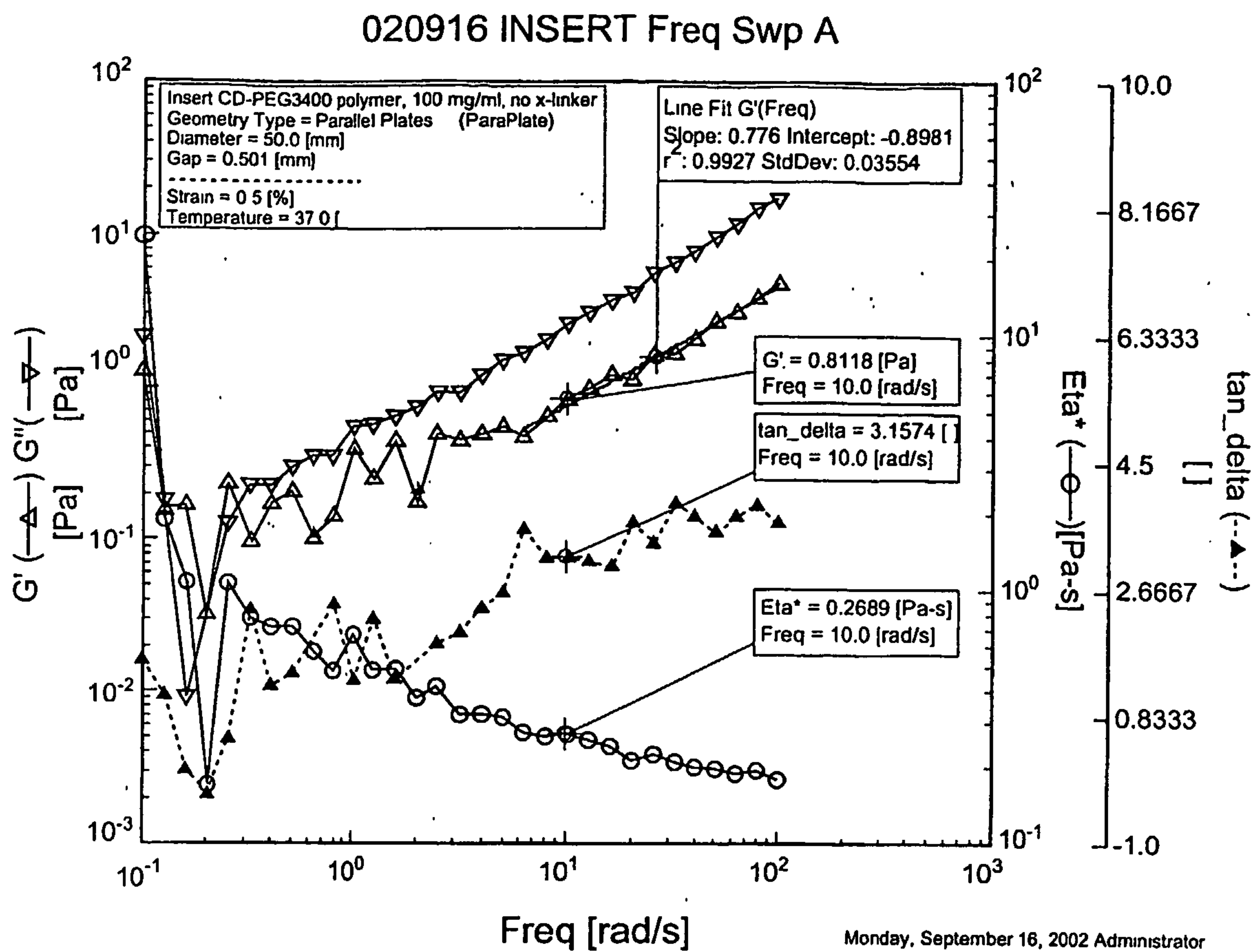


Figure 6

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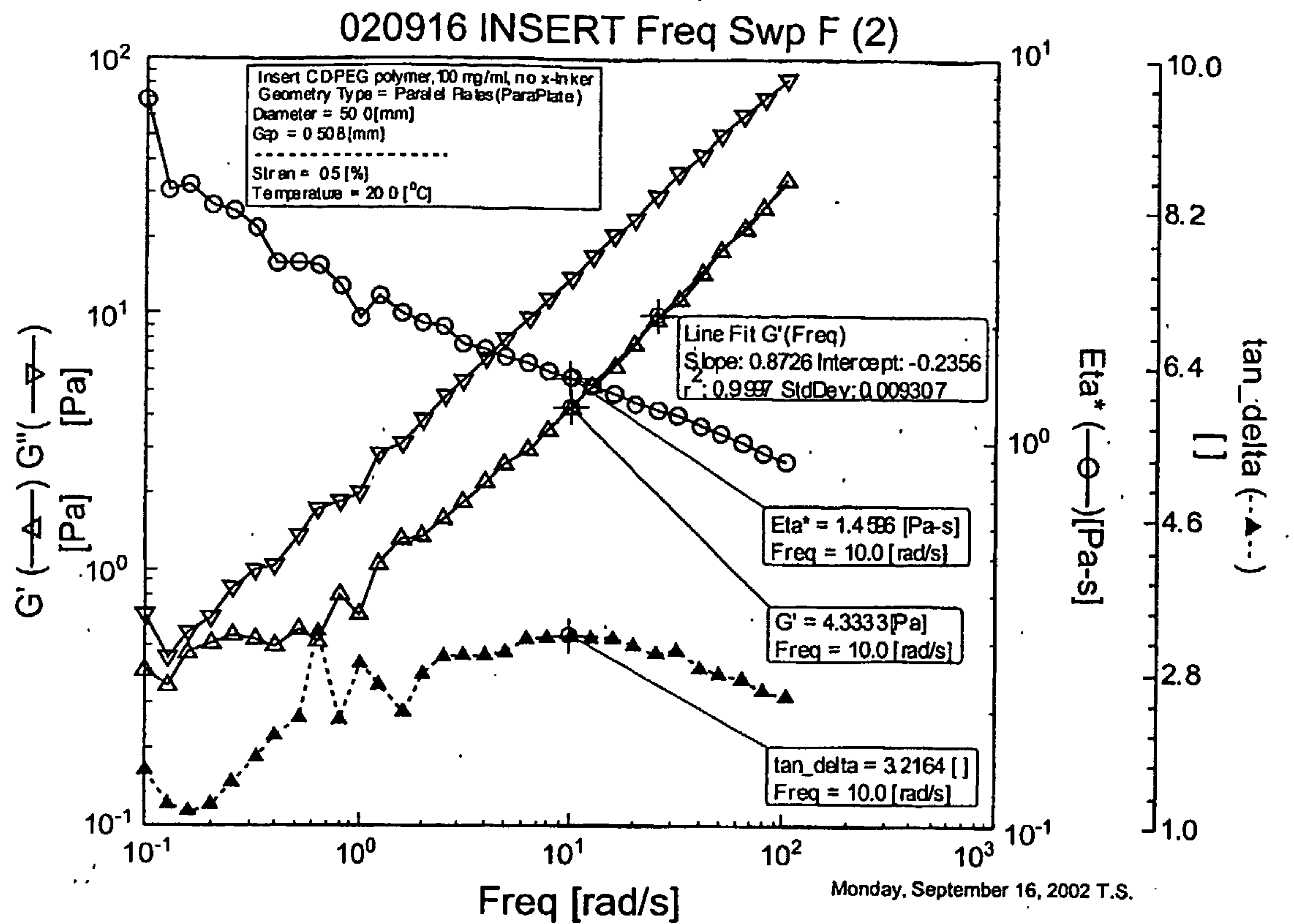


Figure 7

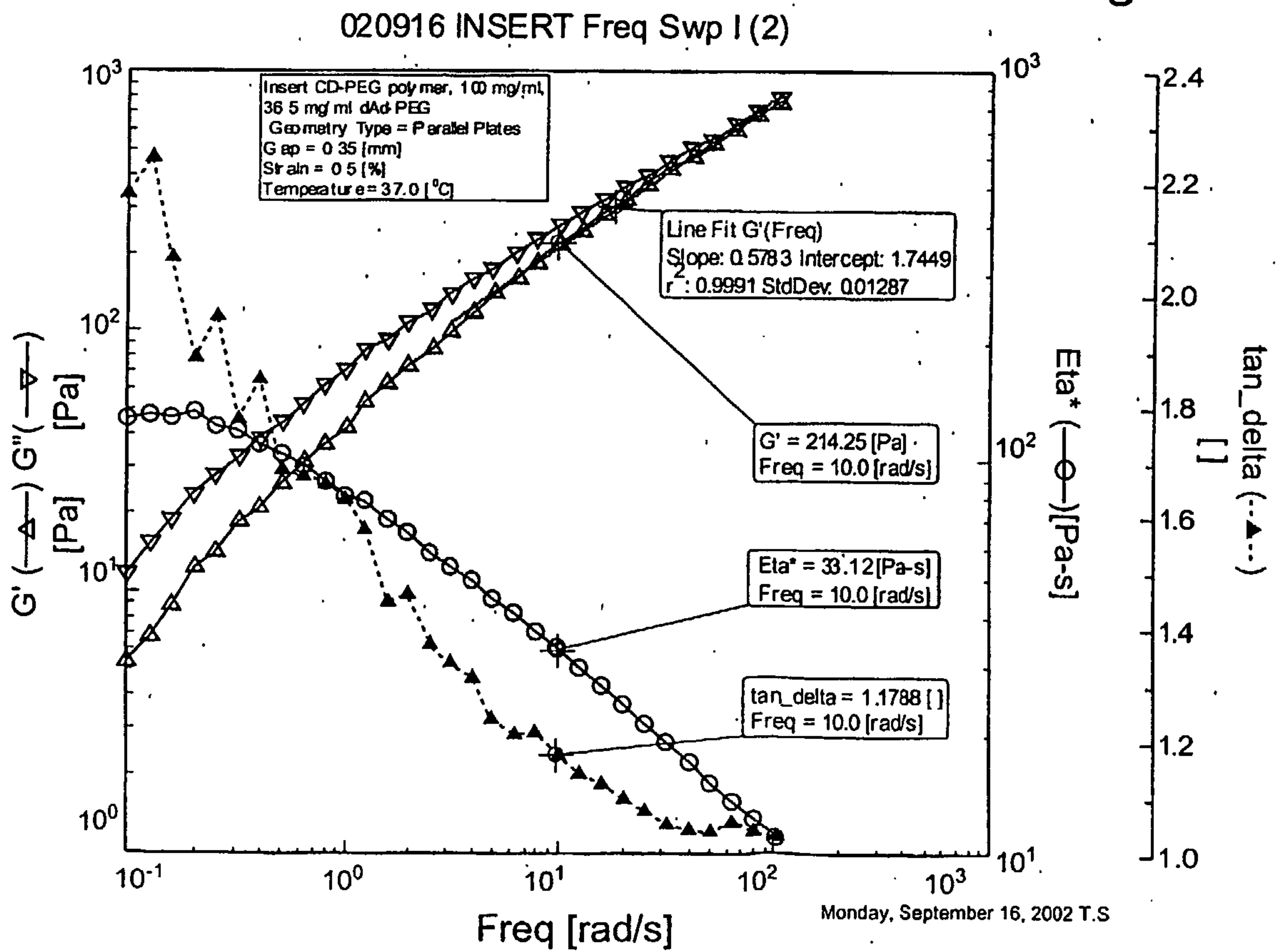


Figure 8

7 / 15

020916 INSERT Freq Swp L

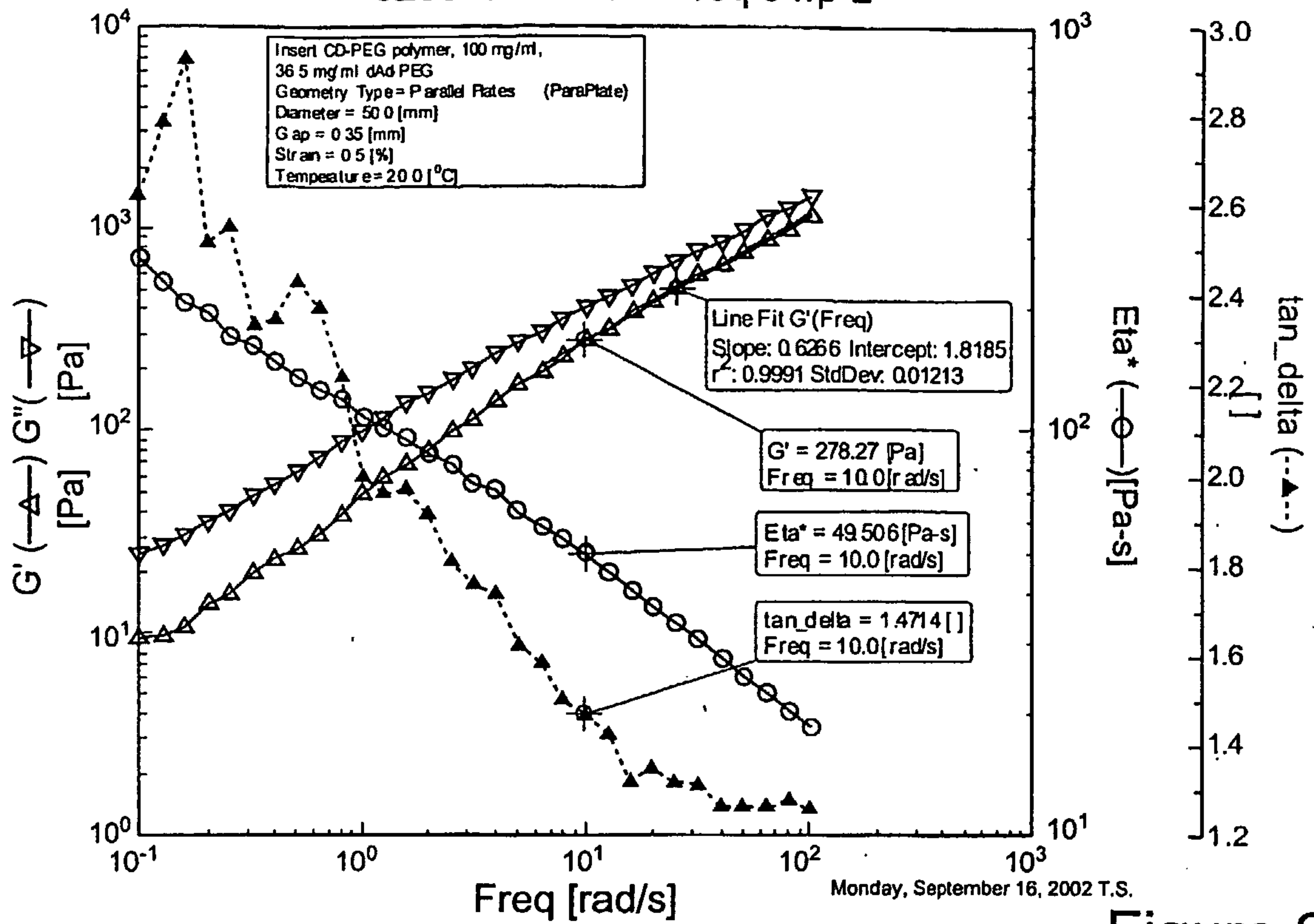


Figure 9

5-24-02 -- Sequence 3 -- 2.4mg -- Trial 3 (SeqTest 2)

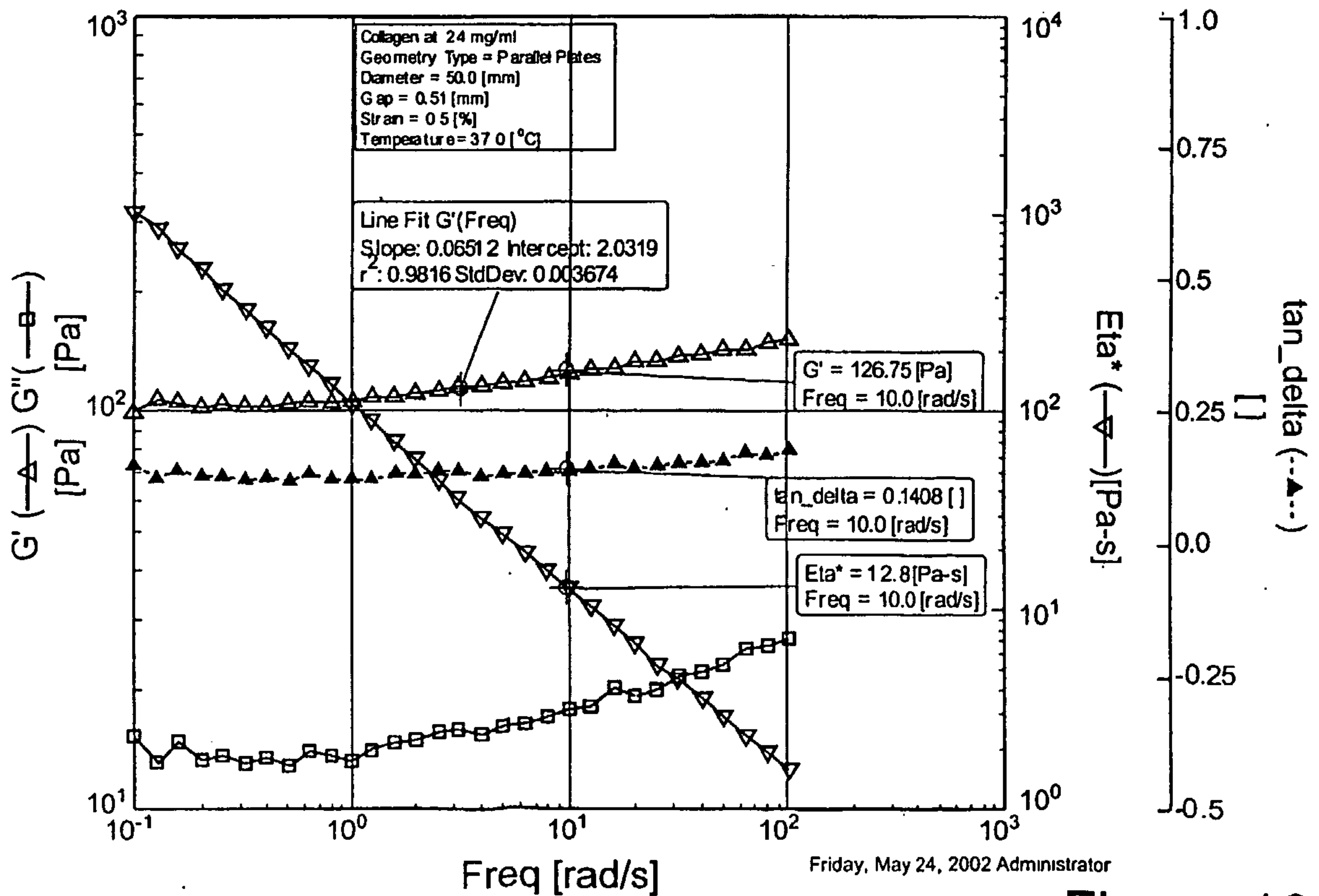


Figure 10

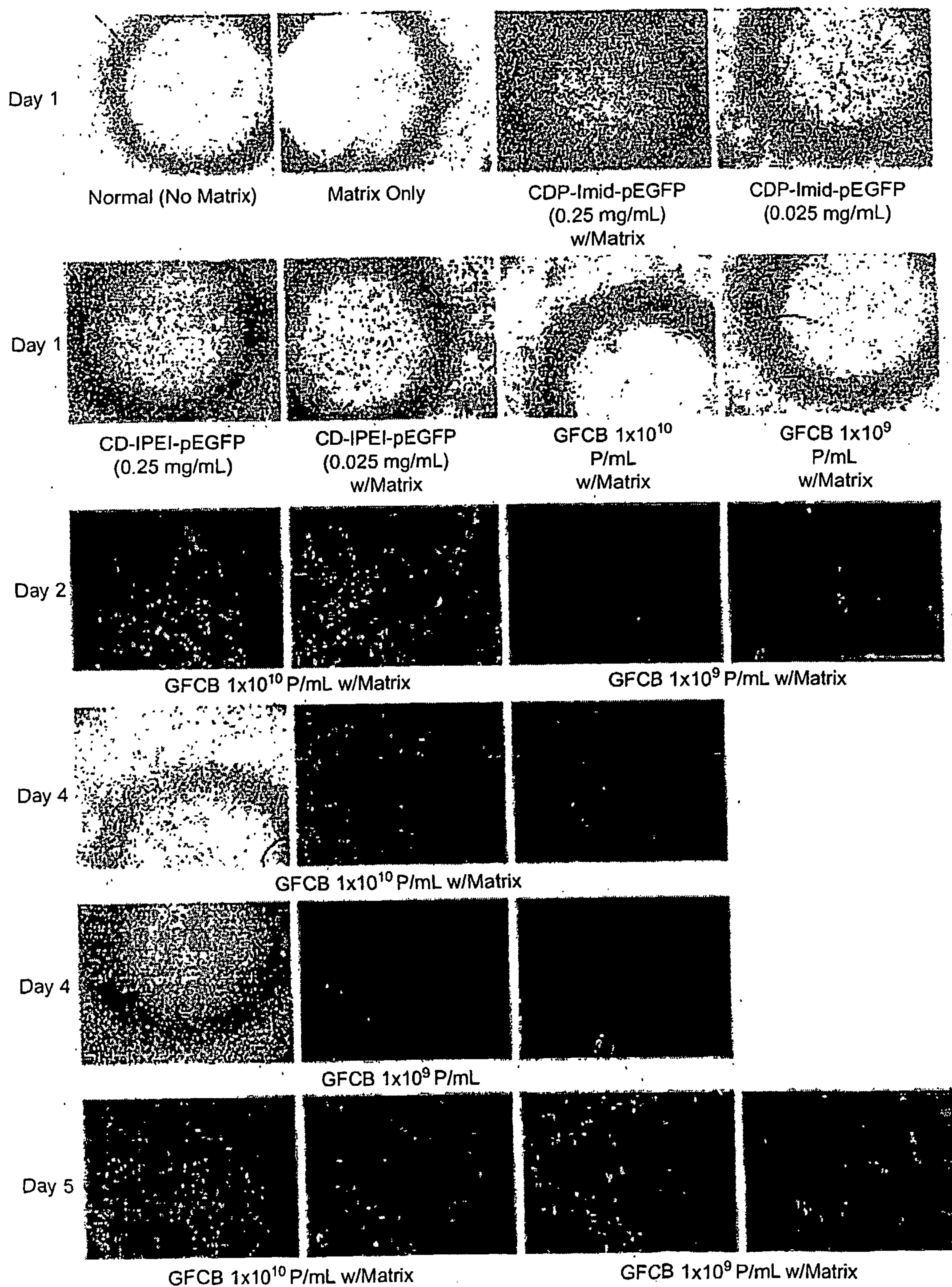


Figure 11

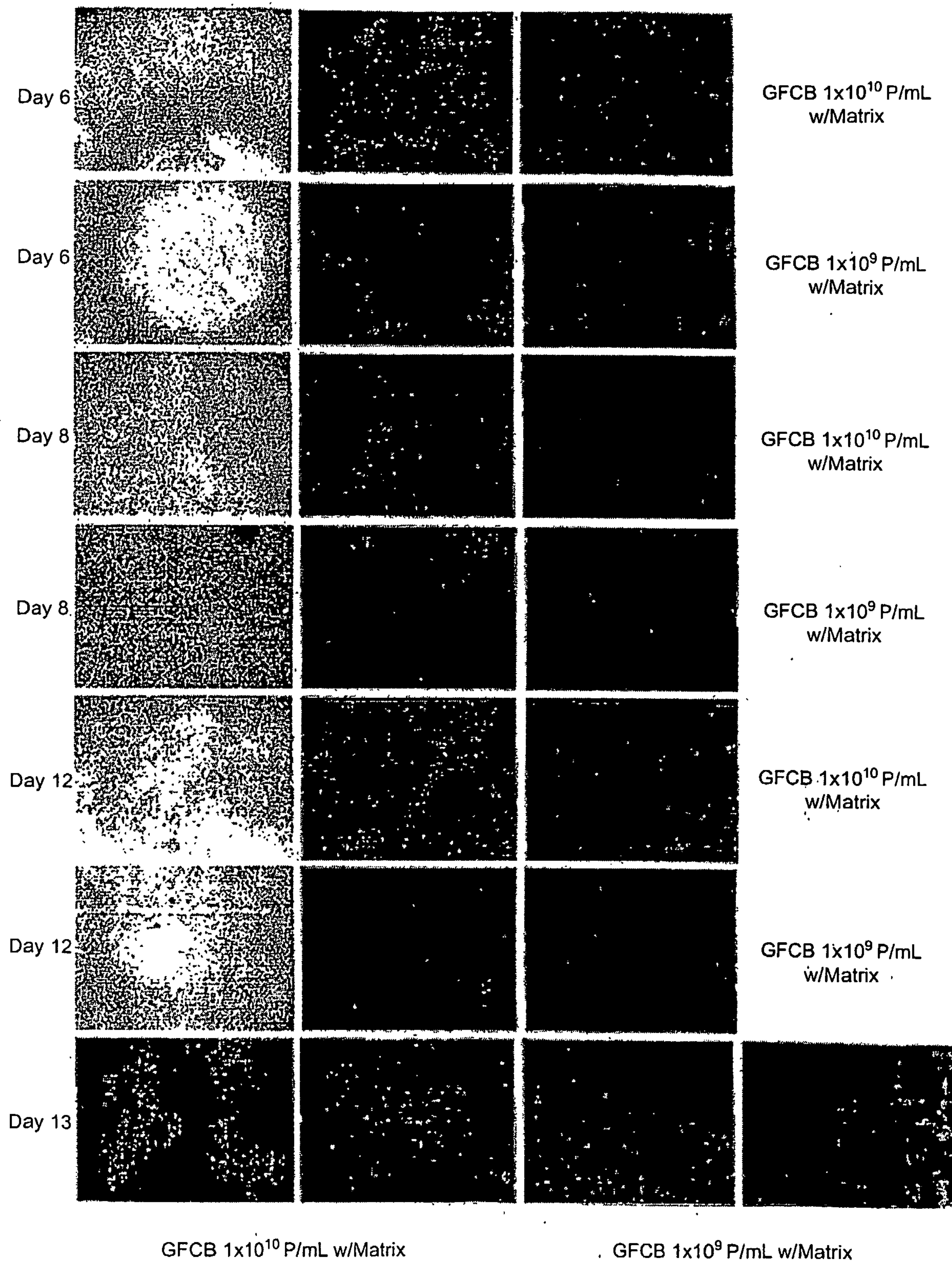
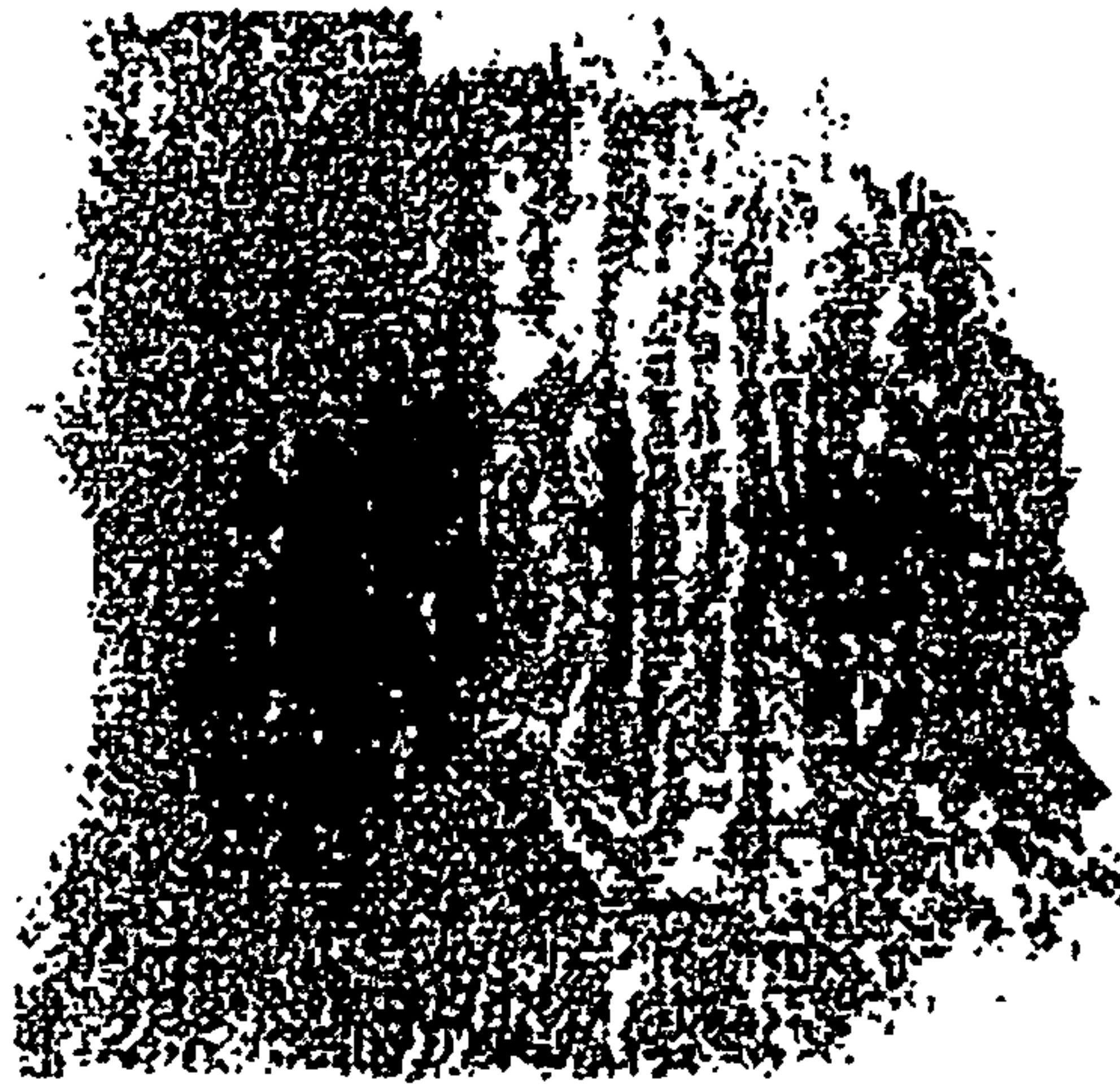


Figure 11 (continued)



A



B

Figure 12



A



B

Figure 13

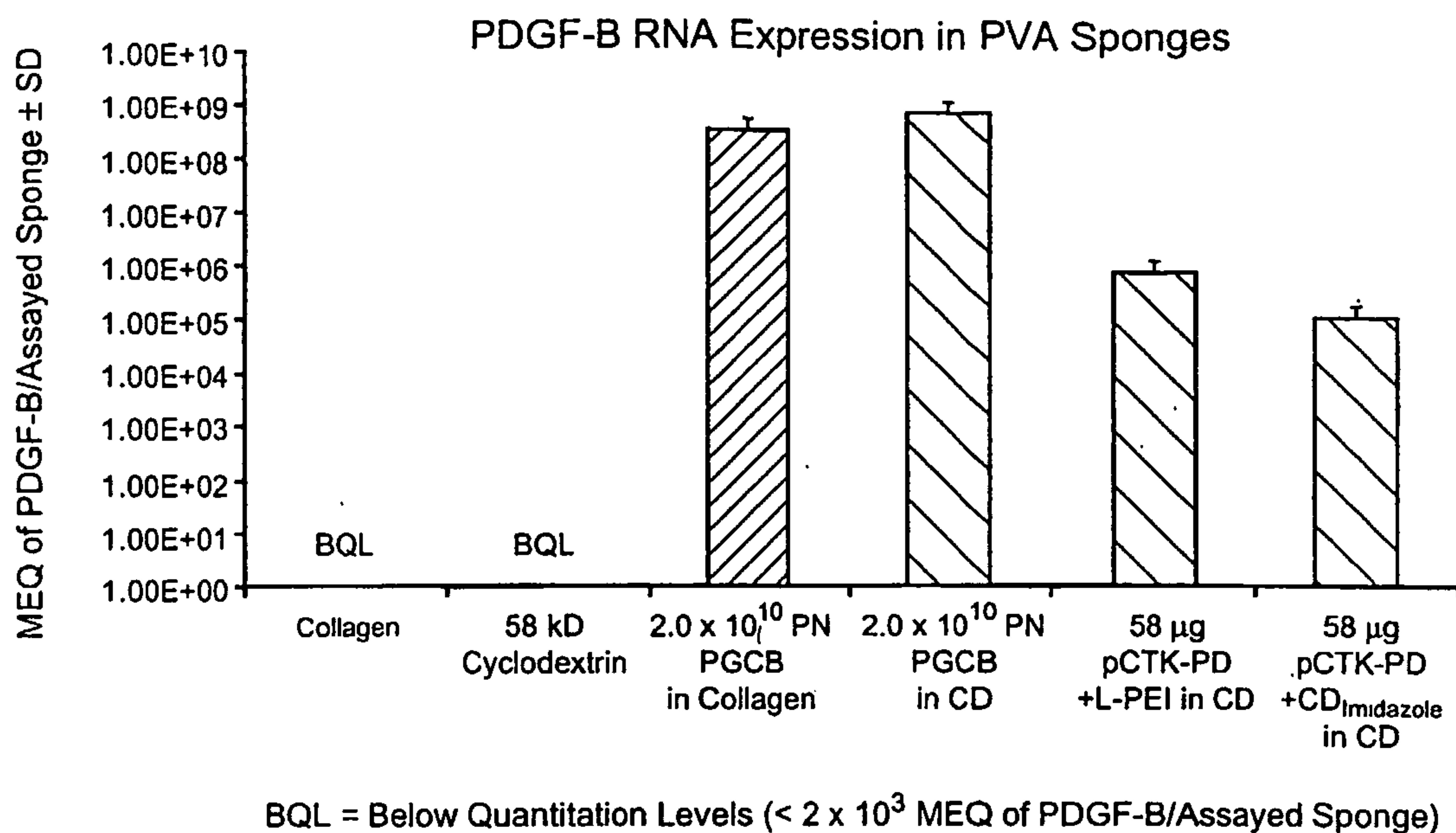


Figure 14

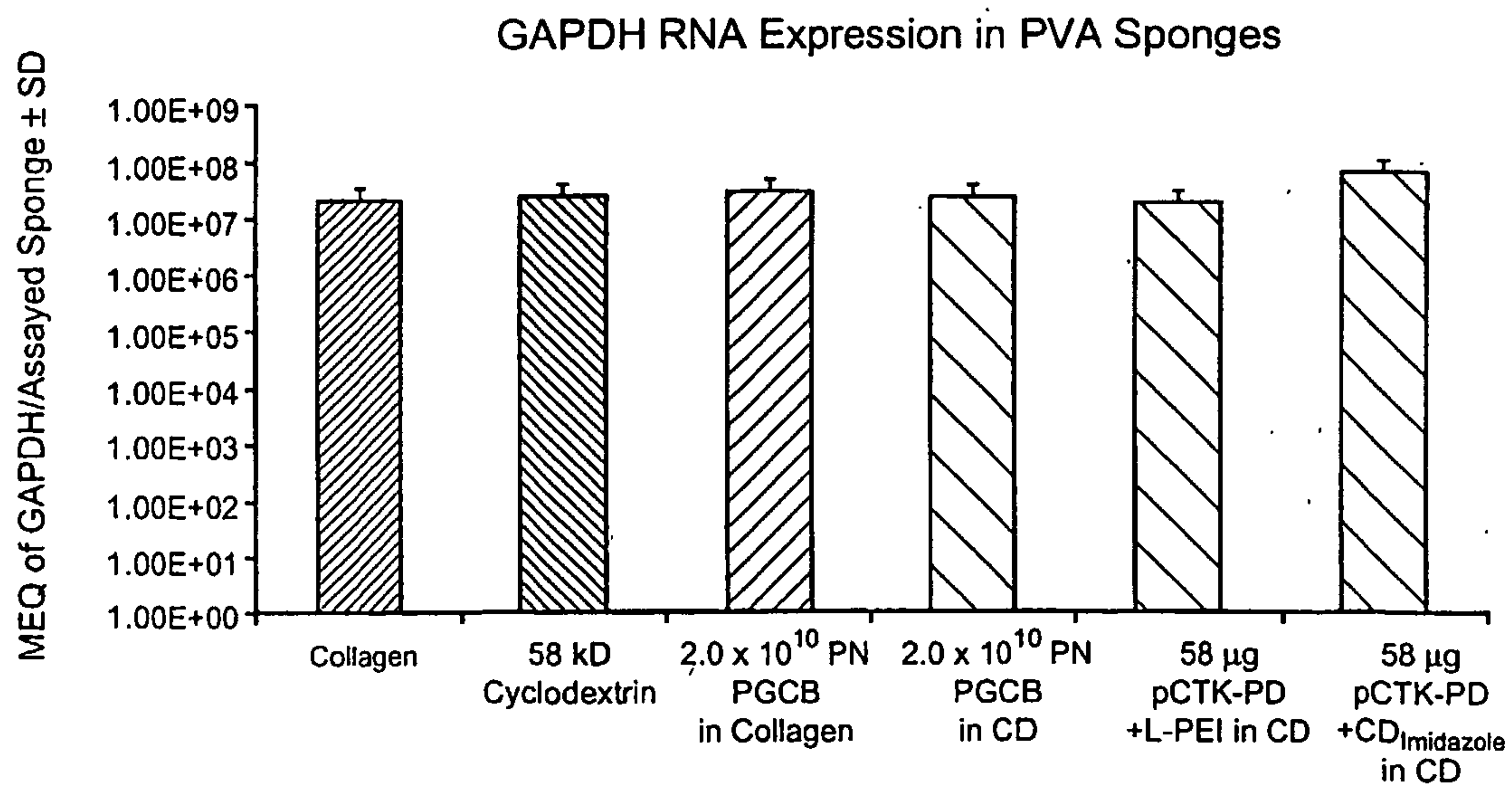


Figure 15

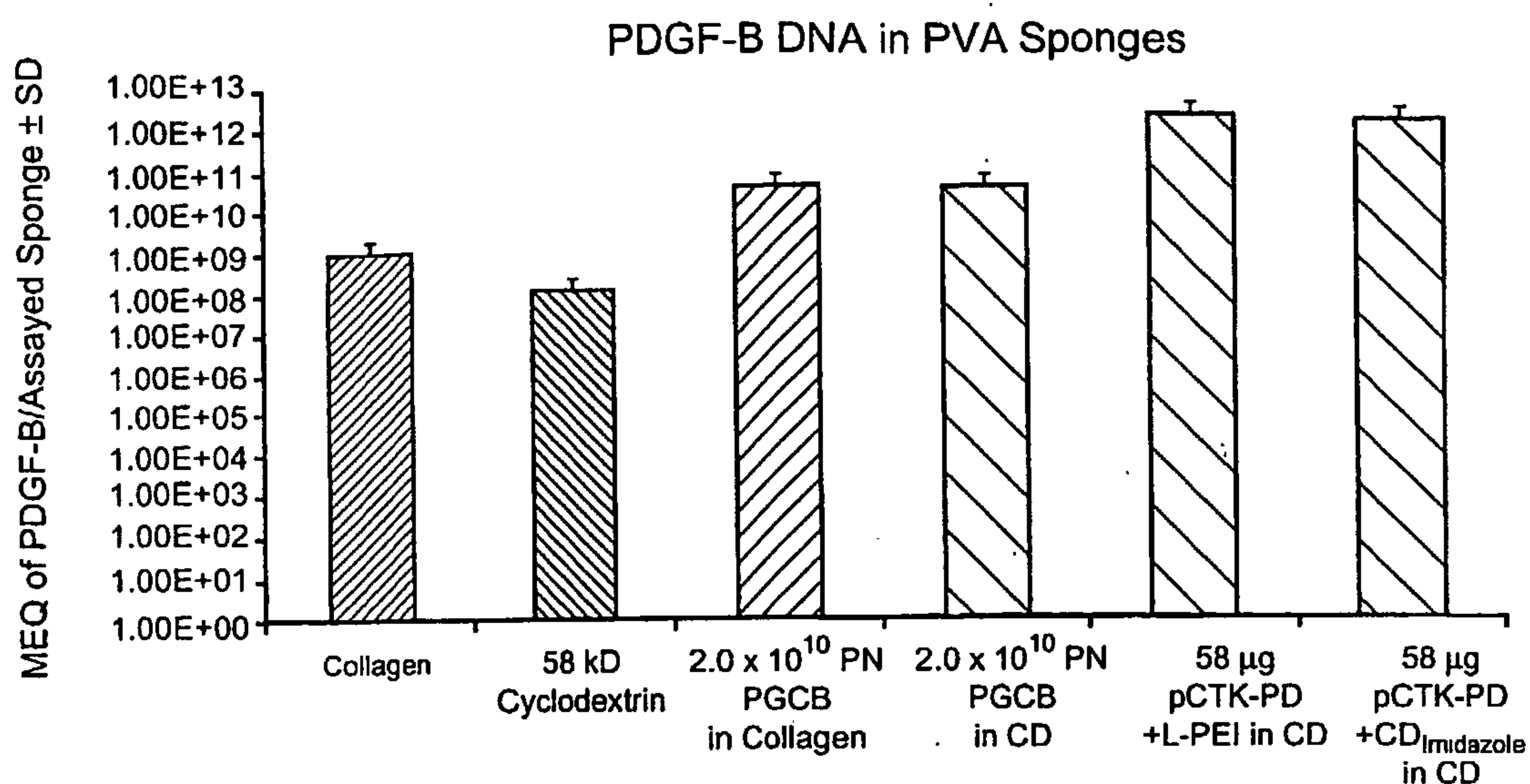


Figure 16

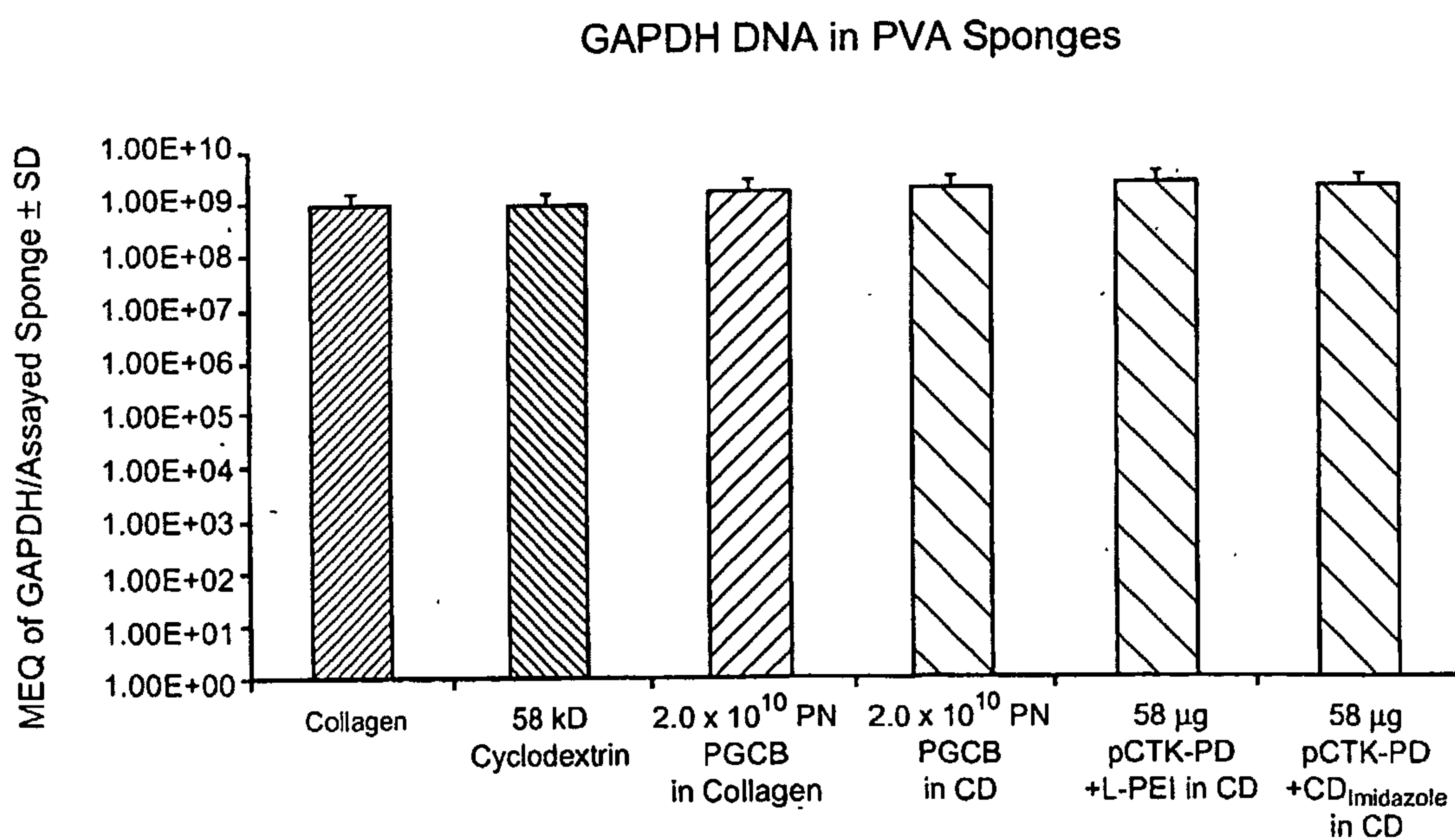
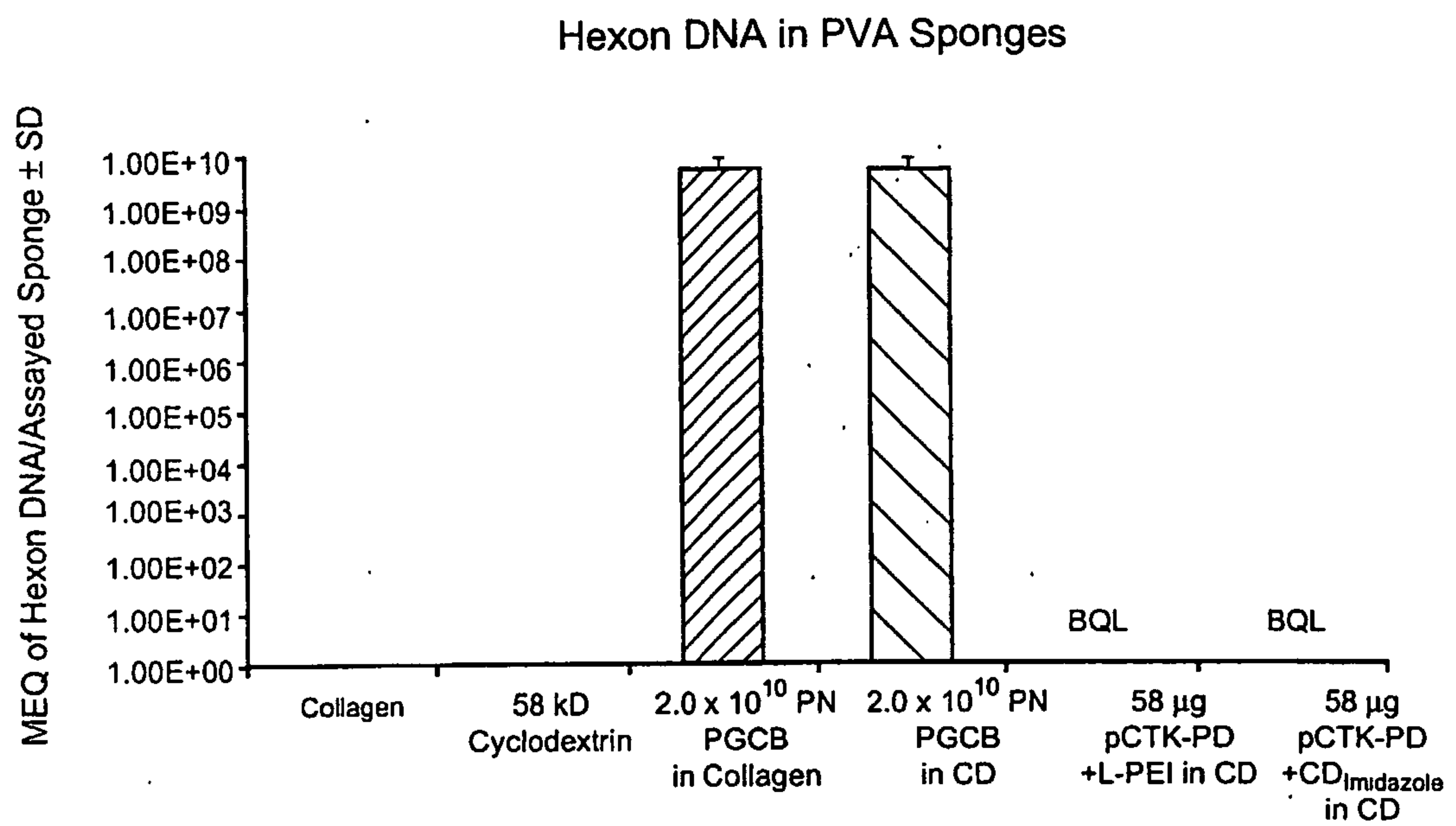


Figure 17

**Figure 18**

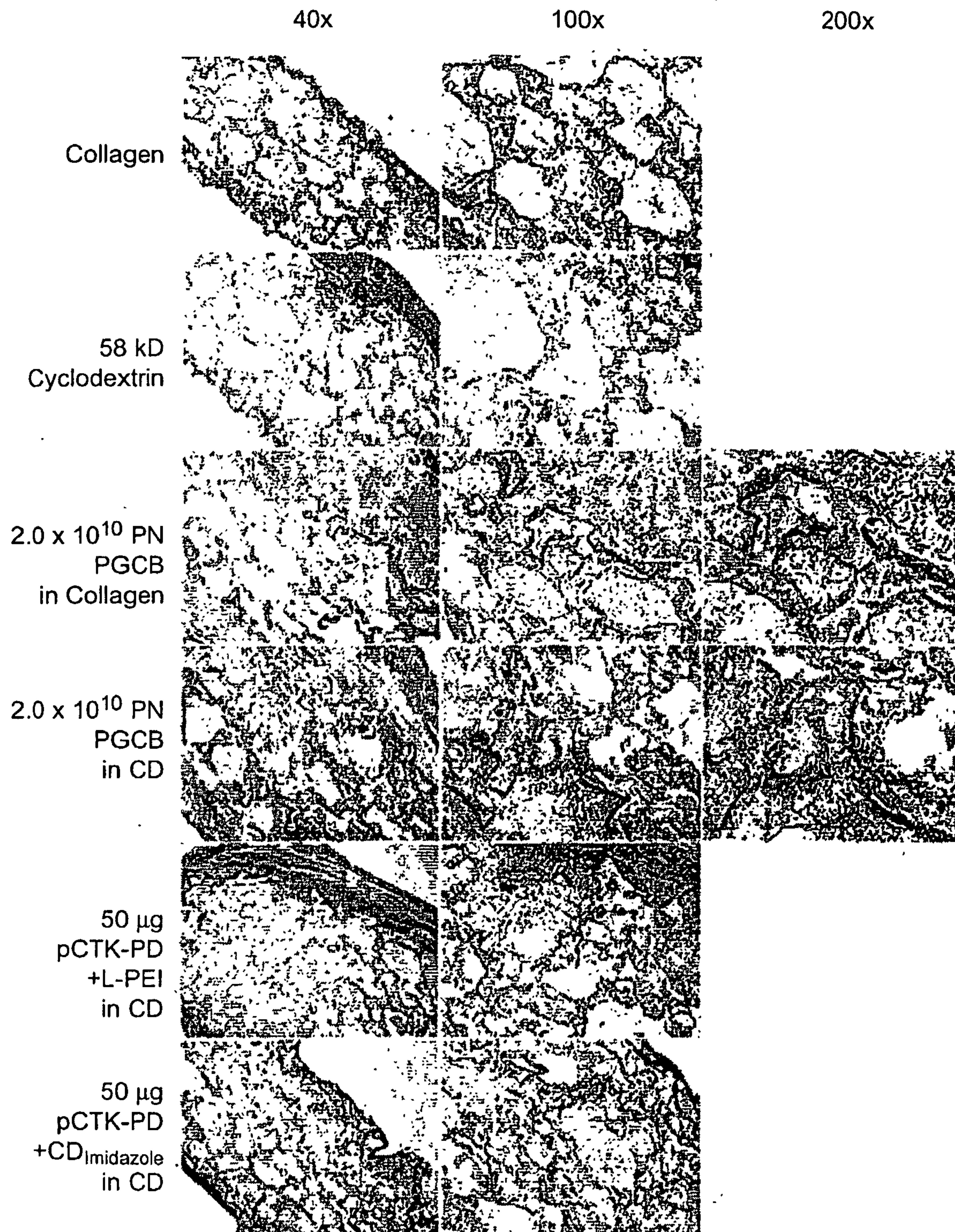


Figure 19