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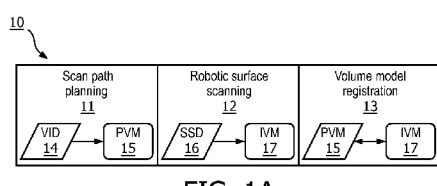
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FIG. 1A

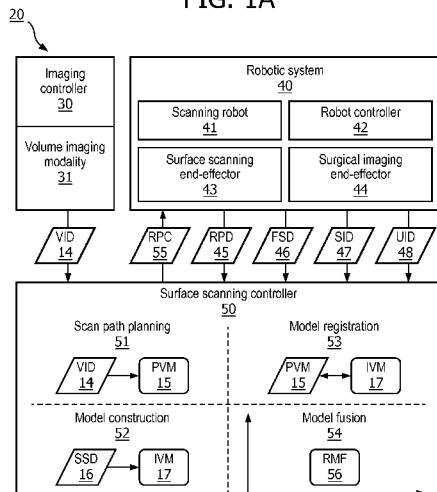


FIG. 1B

(57) Abstract: A force sensed surface scanning system (20) employs a scanning robot (41) and a surface scanning controller (50). The scanning robot (41) includes a surface scanning end-effector (43) for generating force sensing data informative of a contact force applied by the surface scanning end-effector (43) to an anatomical organ. In operation, the surface scanning controller (50) controls a surface scanning of the anatomical organ by the surface scanning end-effector (43) including the surface scanning end-effector (43) generating the force sensing data, and further constructs an intraoperative volume model of the anatomical organ responsive to the force sensing data generated by the surface scanning end-effector (43) indicating a defined surface deformation offset of the anatomical organ.

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FORCE SENSED SURFACE SCANNING SYSTEMS, DEVICES, CONTROLLERS AND METHODS

FIELD OF THE INVENTION

5 The inventions of the present disclosure generally relate to systems, devices, controllers and methods for a surface scanning of an anatomical organ (e.g., a liver, a heart, a lung, a brain, a stomach, a spleen, a kidney, a pancreas, a bladder, etc.) for purposes of registering an intraoperative surface scanned volume model of the anatomical organ with a preoperative image segmented volume model of the
10 anatomical organ.

The inventions of the present disclosure more particularly relate to improving such systems, devices, controllers and methods by implementing a force sensing technology into a robotic-assisted surface scanning of an anatomical organ to thereby enhance a registration of an intraoperative surface scanned volume model of the
15 anatomical organ with a preoperative image segmented volume model of the anatomical organ.

BACKGROUND OF THE INVENTION

Minimally invasive surgical operations may be performed through small, single incision ports in the insufflated abdominal wall. Therefore a line-of-sight via an
20 endoscope to surgical instruments and an outer surface of anatomical organ(s) is provided by endoscopic images. Internal structures of the anatomical organ(s) (e.g., vessels, tumors, etc.) are usually visualized with two-dimensional (“2D”) laparoscopic ultrasound (LUS). However, LUS is difficult to interpret in a large anatomical context, especially when the image quality is obscured by tissue abnormalities (e.g. cirrhosis,
25 fatty structures, etc.), by presence of previous oncological therapy (e.g. thermal ablation, transarterial embolization, etc.) and/or by improper acoustic coupling of the LUS to the anatomical organ(s). To improve intraoperative information, a high quality three-dimensional (“3D”) imaging modality (e.g., a computer-tomography modality (CT), a magnetic resonance imaging modality (MRI), cone-beam CT (CBCT), etc.)
30 may be fused with the laparoscopic images whereby image registration may provide knowledge of tumor location depth, vicinity of critical anatomical structures,

predefined resection plans and other additional information useful for the surgical operation.

5 Several surface based registration techniques are known in art of the present disclosure for fusing the 3D preoperative images with the intraoperative physical space. These techniques estimate an image-to-patient transformation matrix by matching a surface of the anatomy segmented from the 3D preoperative images with a sparse representation of the same surface acquired during the procedure.

10 Current techniques as known in the art for intraoperative surface scanning of soft tissue anatomical structure(s) during a surgical procedure utilize either a pre-calibrated tool pointer tracked by external position measurement systems (e.g., optical tracking, electromagnetic tracking, etc.), or external laser range scanners, or 3D multi-view reconstruction from endoscopic images. However, such intraoperative surface scanning is challenging due to unknown tissue properties and large tissue deformation.

15 More particularly, an accurate anatomy scanning using tracked tool pointers is time-consuming and highly user-dependent. The reproducibility of this method is also hindered by tool calibration and tracking system inaccuracies, errors introduced by the operator when maintaining both constant pressure and contact with the organ surface, and unknown deformation of the soft tissue anatomy during the acquisition.

20 On the other hand, laser scanning methods require external laser range scanners, which are difficult to integrate into minimally invasive surgical suite, and are inaccurate due to the reflective nature of the organ's surface.

25 Further a multi-view 3D reconstruction from endoscopic images requires a surface that presents either unique features or the texture and a surface that is not covered by blood.

SUMMARY OF THE INVENTION

To improve upon surface scanning systems, devices, controllers and methods for intraoperative surface scanning of soft tissue anatomical structure(s) during a surgical procedure, the present disclosure provides inventions for constructing an 30 intraoperative scanned volume model of an anatomical organ based upon a sensing of a contact force applied by a surface scanning end-effector of a scanning robot to the

anatomical organ whereby the contact force is indicative of a defined surface deformation offset of the anatomical organ.

One embodiment of the inventions of the present disclosure is a force sensed surface scanning system employing a scanning robot and a surface scanning controller.

5 The scanning robot includes a surface scanning end-effector for generating force sensing data informative of a contact force applied by the surface scanning end-effector to an anatomical organ.

The surface scanning controller is employed for controlling a surface scanning of the anatomical organ by the surface scanning end-effector including the surface 10 scanning end-effector generating the force sensing data, and for constructing a intraoperative volume model of the anatomical organ responsive to the force sensing data generated by the surface scanning end-effector indicating a defined surface deformation offset of the anatomical organ.

15 A second embodiment of the inventions of the present disclosure is the surface scanning controller employing a scanning commander (133) and a model constructor (134).

The scanning commander (133) is employed for controlling the surface scanning of the anatomical organ by the surface scanning end-effector including the surface scanning end-effector generating force sensing data informative of the contact 20 force applied by the surface scanning end-effector to the anatomical organ.

The model constructor (134) is employed for constructing the intraoperative volume model of the anatomical organ responsive to the force sensing data generated by the surface scanning end-effector indicating a defined surface deformation offset of the anatomical organ.

25 A third embodiment of the inventions of the present disclosure is a force sensed surface scanning method involving the surface scanning controller controlling a surface scanning of an anatomical organ by the surface scanning end-effector scanning end-effector including the surface scanning end-effector generating force sensing data informative of a contact force applied by the surface scanning end-effector to the 30 anatomical organ.

The force sensed surface scanning method further involves surface scanning controller constructing a intraoperative volume model of the anatomical organ

responsive to the force sensing data generated by the surface scanning end-effector indicating a defined surface deformation offset of the anatomical organ.

For purposes of describing and claiming the inventions of the present disclosure:

5 (1) terms of the art of the present disclosure including, but not limited to, “imaging modality”, “scanning robot” and “end-effector” are to be understood as known in the art of the present disclosure and exemplary described herein;

10 (2) the term “force sensed surface scanning system” broadly encompasses all surface scanning systems, as known in the art of the present disclosure and hereinafter conceived, incorporating the inventive principles of the present disclosure for implementing a force sensing technology into a robotic-assisted surface scanning of an anatomical organ. Examples of known surface scanning systems include, but are not limited to, Philips augmented-reality surgical navigation systems, Philips L10-4lap linear transducer based systems, BrainLab Cranial navigation with navigated pointer

15 tool for surface digitalization, and Pathfindeer surgical navigation system;

20 (3) the term “force sensed surface scanning method” broadly encompasses all surface scanning methods, as known in the art of the present disclosure and hereinafter conceived, incorporating the inventive principles of the present disclosure for implementing a force sensing technology into a robotic-assisted surface scanning of an anatomical organ. A non-limiting example of a known surface scanning method is Philips Pinnacle3;

25 (4) the term “controller” broadly encompasses all structural configurations of an application specific main board or an application specific integrated circuit for controlling an application of various inventive principles of the present disclosure related to monitoring a folding and/or a twisting of an interventional device within the anatomical lumen as subsequently exemplarily described herein. The structural configuration of the controller may include, but is not limited to, processor(s), computer-readable/computer readable storage medium(s), an operating system, application module(s), peripheral device controller(s), interface(s), bus(es), slot(s) and

30 port(s). The labels “imaging”, “robot” and “surface scanning” as used herein for the term “controller” distinguishes for identification purposes a particular controller from

other controllers as described and claimed herein without specifying or implying any additional limitation to the term “controller”.

(6) the term “application module” broadly encompasses a component of an controller consisting of an electronic circuit and/or an executable program (e.g., executable software and/or firmware stored on non-transitory computer readable medium(s)) for executing a specific application. The labels “scanning commander”, “model constructor”, “model registor” and “model fuser” as used herein for the term “module” distinguishes for identification purposes a particular module from other modules as described and claimed herein without specifying or implying any additional limitation to the term “application module”; and

(7) the terms “data”, and “command” broadly encompasses all forms of a detectable physical quantity or impulse (e.g., voltage, current, or magnetic field strength) as understood in the art of the present disclosure and as exemplary described herein for communicating information and/or instructions in support of applying various inventive principles of the present disclosure as subsequently described herein. Data/command communication between components of the present disclosure may involve any communication method, as known in the art of the present disclosure and hereinafter conceived, including, but not limited to, data/command transmission/reception over any type of wired or wireless medium/datalink and a reading of data/command uploaded to a computer-usuable/computer readable storage medium.

The foregoing embodiments and other embodiments of the inventions of the present disclosure as well as various features and advantages of the inventions of the present disclosure will become further apparent from the following detailed description of various embodiments of the inventions of the present disclosure read in conjunction with the accompanying drawings. The detailed description and drawings are merely illustrative of the inventions of the present disclosure rather than limiting, the scope of the inventions of the present disclosure being defined by the appended claims and equivalents thereof.

FIG. 1A illustrates an exemplary embodiment of a force sensed surface scanning method in accordance with the inventive principle of the present disclosure.

FIG. 1B illustrates an exemplary embodiment of a force sensed surface scanning system in accordance with the inventive principle of the present disclosure.

FIGS. 2A and 2B illustrate exemplary scanned path planning in accordance with the inventive principles of the present disclosure.

5 FIGS. 3A-3C illustrate an exemplary surface scanning of an anatomical organ by a surface scanning end-effector in accordance with the inventive principle of the present disclosure.

10 FIG. 4 illustrates an exemplary embodiment of the force sensed surface scanning system of FIG. 1B in accordance with the inventive principle of the present disclosure.

FIG. 5 illustrates a flowchart representative of an exemplary embodiment of the force sensed surface scanning method of FIG. 1A in accordance with the inventive principle of the present disclosure.

15 FIGS. 6A-6F illustrate an exemplary surface scanning of an anatomical organ by a pointer tool in accordance with the inventive principle of the present disclosure.

FIGS. 7A-7F illustrate an exemplary surface scanning of an anatomical organ by a ultrasound laparoscope in accordance with the inventive principle of the present disclosure.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

20 As an improvement of known surface scanning systems, devices, controllers and methods for intraoperative surface scanning of soft tissue anatomical organ(s) during a surgical procedure, the present disclosure provides inventions for constructing an intraoperative scanned volume model of an anatomical organ based upon a sensing of a contact force applied by an surface scanning end-effector of a scanning robot to the 25 anatomical organ whereby the contact force is indicative of a defined surface deformation offset of the anatomical organ.

To facilitate an understanding of the various inventions of the present disclosure, the following description of FIGS. 1A and 1B teaches embodiments of a force sensed surface scanning method 10 and a force sensed surface scanning system 30 20 in accordance with the inventive principles of the present disclosure. From this description, those having ordinary skill in the art will appreciate how to practice various and numerous embodiments of force sensed surface scanning methods and force sensed

surface scanning systems in accordance with the inventive principles of the present disclosure.

Also from this description, those having ordinary skill in the art will appreciate an application of the force sensed surface scanning methods and force sensed surface scanning systems of the present disclosure in support of surgical procedures utilizing fusion of preoperative imaging and intraoperative imaging. Examples of such surgical procedure include, but are not limited to, a cardio-thoracic surgery, a prostatectomy, a splenectomy, a nephrectomy and a hepatectomy.

Referring to FIG. 1B, force sensed surface scanning system 20 employs a volume imaging modality 30, a robotic system 40 and a surface scanning controller 50.

Volume imaging modality 31 is an imaging modality for generating a preoperative volume image of an anatomical region as known in the art of the present disclosure (e.g., a computed tomography imaging, a magnetic resonance imaging, an ultrasound imaging modality, a positron emission tomography imaging, and a single photo emission computed tomography imaging of a thoracic region, a cranial region, an abdominal region or a pelvic region).

Robotic system 40 employs a scanning robot 41, a robot controller 42, a surface scanning end-effector 43 and an ultrasound imaging end-effector 44.

A scanning robot 41 is any type of robot, known in the art of the present disclosure or hereinafter conceived, that is structurally configured or structurally configurable with one or more end-effectors utilized in the performance of a surgical procedure. Further, scanning robot 41 is equipped with pose tracking technology and force sensing technology as known in the art of the present disclosure.

In one exemplary embodiment, a scanning robot 41 is a snake scanning robot equipped with a rotary encoder embedded in each joint of the snake scanning robot for tracking a pose of the snake scanning robot as known in the art of the present disclosure, and further equipped with a force sensor, a pressure sensor, or an optical fiber for sensing a contact force between an end-effector of the snake scanning robot and an anatomical organ as known in the art of the present disclosure.

Robot controller 42 controls a pose of scanning robot 41 within a relevant coordinate system in accordance with robot position commands 55 issued by surface scanning controller 50 as known in the art of the present disclosure.

Surface scanning end-effector 43 is utilized to construct an intraoperative scanned volume model 15 of the anatomical region in accordance with the inventive principles of the present invention as will be further explained herein. In practice, surface scanning end-effector 43 may be any type of end-effector having a calibration scan reference thereon as known in the art of the present disclosure. In exemplary embodiments, surface scanning end-effector 43 may include mount holding a tool pointer having a spherical distal tip serving as a calibrated scanning reference, or may include a mount holding an ultrasound laparoscope having an ultrasound transducer serving as a calibrated scanning reference.

10 Surgical imaging end-effector 44 is utilized to intraoperatively image an external surface and/or internal structures within the anatomical organ in support of a surgical procedure as known in the present disclosure. In an exemplary embodiment, surgical imaging end-effector 44 may be an ultrasound laparoscope, which may also serve as surface scanning end-effector 43.

15 In practice, surface scanning end-effector 43 is mounted onto scanning robot 41 whereby robot controller 42 controls scanning robot 41 in accordance with robot position commands 55 from surface scanning controller 50 to implement a robotic surface scanning 12 of force sensed surface scanning method 10 of FIG. 1A as will be further explained herein. Subsequently, surgical imaging end-effector 44 is mounted 20 onto scanning robot 41 whereby robot controller 42 controls scanning robot 41 in accordance with interactive or planned commands from an operator of robotic system 40 during a surgical procedure as will be further explained herein.

25 Alternatively in practice, surface scanning end-effector 43 is affixed to scanning robot 41 whereby robot controller 42 controls scanning robot 41 in accordance with robot position commands 55 from surface scanning controller 50 to implement a robotic surface scanning 12 of force sensed surface scanning method 10 of FIG. 1A as will be further explained herein. Subsequently, surgical imaging end-effector 44 is affixed to or mounted onto an additional scanning robot 41 whereby robot controller 42 controls the additional scanning robot 41 in accordance with interactive or planned 30 commands from an operator of robotic system 40 during a surgical procedure as will be further explained herein.

Surface scanning controller 50 controls an implementation of force sensed surface scanning method 10 (FIG. 1A) of the present disclosure as will now be described herein.

Referring to FIGS. 1A and 1B, force sensed surface scanning method 10 5 involves a scan path planning phase 11, a robotic surface scanning phase 12 and a volume model registration phase 13.

Prior to a path planning phase 11 of method 10, an imaging controller 30 is 10 operated for controlling a generation by a volume imaging modality 31 of a preoperative volume image of an anatomical region as known in the art of the present disclosure (e.g., a computed tomography imaging, a magnetic resonance imaging, an ultrasound imaging modality, a positron emission tomography imaging, and a single photo emission computed tomography imaging of a thoracic region, a cranial region, an abdominal region and a pelvic region).

Path planning phase 11 of method 10 encompasses a communication of volume 15 image data 14 representative of the preoperative volume image of the anatomical organ to surface scanning controller 50 by any communication technique known in the art of the present disclosure (e.g., a data upload or a data streaming). Surface scanning controller 50 processes volume image data 14 to generate a preoperative image segmented volume model 15 of an anatomical organ within the anatomical region as 20 known in the art of the present disclosure (e.g., a segmented volume model of a liver, a heart, a lung, a brain, a stomach, a spleen, a kidney, a pancreas, a bladder, etc.).

Alternatively, imaging controller 30 may processes volume image data 14 to 25 generate preoperative image segmented volume model 15 of the anatomical organ as known in the art of the present disclosure whereby path planning phase 11 of method 10 encompasses a communication of preoperative image segmented volume model 15 of the anatomical organ to surface scanning controller 50 by any communication technique known in the art of the present disclosure (e.g., a data upload or a data streaming).

Path planning phase 11 of method 10 further encompasses surface scanning 30 controller 50 executing a scan path planning 51 involving a definition of a path along one or more segments or an entirety of a surface of preoperative image segmented volume model 15 of the anatomical organ as known in the art of the present disclosure.

In one embodiment of scan path planning 51, surface scanning controller 50 implements an operator or systematic delineation as known in the art of the present disclosure of a line sampling scan path on preoperative image segmented volume model 15 of the anatomical organ involving a continuous contact between surface scanning 5 end-effector 43 and the anatomical organ as surface scanning end-effector 42 is traversed along one or more lines over a surface segment or an entire surface of preoperative image segmented volume model 15 of the anatomical organ.

For example, FIG. 2A illustrates an exemplary delineation of a line sampling 10 scan path 15a including a plurality of lines traversing the surface of a preoperative image segmented volume model of a liver. In practice, the lines may be disconnected as shown or connected to any degree by an operator or system delineation of path 15a.

Alternatively in practice, a line sampling scan path may be defined independent 15 of the preoperative image segmented volume. For example, the line sampling scan path may be a defined as a geometric pattern (e.g., a spiral pattern, a zigzag pattern, etc.) or as a random pattern (e.g., a white noise sampling scheme) or a combination thereof.

In a second embodiment of scan path planning 51, surface scanning controller 50 implements an operator or systematic delineation as known in the art of the present disclosure of a point sampling scan path on preoperative image segmented volume model 15 of the anatomical organ involving a periodic contact between surface 20 scanning end-effector 43 and the anatomical organ as surface scanning end-effector 42 is traversed over a surface segment or an entire surface of preoperative image segmented volume model 15 of the anatomical organ.

For example, FIG. 2B illustrates an exemplary a delineation of a point sampling 25 scan path 15b including a plurality of points marked on a surface of a preoperative image segmented volume model of a liver. In practice, as designed by an operator or system delineation of path 15b, the points may be arranged in an uniform pattern as shown or in a non-uniform pattern.

Alternatively in practice, a point sampling scan path may be defined 30 independent of the preoperative image segmented volume. For example, the line sampling scan path may be a defined as a geometric pattern (e.g., a spiral pattern, a zigzag pattern, etc.) or as a random pattern (e.g., a white noise sampling scheme) or a combination thereof.

Further in practice, scan path planning 51 may also involve any combination of a line sampling scan path and a point sampling scan path delineated on preoperative image segmented volume model 15 of the anatomical organ.

5 Additionally in practice, scan path planning 51 may be omitted for surface scanning controller 50 or not used by surface scanning controller 50 for a particular procedure. In this scenario, an operator of system 20 may control a navigation of scanning robot 41 in implementing an operator defined sampling scan path.

10 Still referring to FIGS. 1A and 1B, robotic surface scanning phase 12 of method 10 encompasses an image guidance of surface scanning end-effector 43 in proximity of the anatomical organ whereby surface scanning controller 50 is operated to issue robot position commands 55 to robot controller 42 for controlling a navigation of surgical scanning end-effector 43 relative to the anatomical organ in accordance with the planned sampling scan path delineated on preoperative image segmented volume model 15 of the anatomical organ.

15 More particularly, to facilitate a model registration 53 in accordance with the inventive principles of the present disclosure as will be further described herein, robotic system 40 communicates surface sensing data 16 to surface scanning controller 50 whereby surface scanning controller 50 implements a model construction 52 of an inoperative volume model 17 of the anatomical organ in accordance with the inventive 20 principles of the present disclosure as will be further described herein.

More particularly, surface sensing data 16 includes robotic position data 45 communicated by robot controller 42 to surface scanning controller 50 whereby robot position data 45 is informative of a current pose of scanning robot 41 within a coordinate system registered to the anatomical organ or preoperative segmented volume 25 model as known in the art of the present disclosure.

Surface sensing data 16 further includes force sensing data 46 informative of a contact force applied by the surface scanning end-effector 43 to the anatomical organ, and for imaging embodiments of surface scanning end-effector 43, surface sensing data 16 further includes scan image data 47 representative of a current image slice of the 30 anatomical image.

Surface scanning controller 50 processing robot position data 45, force sensing data 46 and scan image data 47 (if applicable) to construct an inoperative volume

model 17 of the anatomical organ based on a physical behavior of a soft tissue of an anatomical organ under a minor deformation by scanning surface end-effector 42 (e.g., a tissue deformation in nanometers).

Specifically, model construction 52 is premised on an assumption that the physical behaviour soft tissue of an anatomical organ under a minor deformation is both linearly elastic and one-dimensional. Under such conditions, an offset between undeformed anatomical tissue and deformed anatomical tissue may be calculated using the equation $u = f / k$, where u is a tissue displacement (offset), f is the sensed contact force between surface scanning end effector 43 and the deformed anatomical tissue, and k is a parameter describing viscoelastic properties of the anatomical organ.

From the assumption, model construction 52 involves a designation of a defined scanning force parameter f_{DC} and of a defined viscoelastic property parameter k whereby a surface deformation offset u_{SDO} may be calculated to support the construction of the inoperative volume model 17 of the anatomical organ as will be further explained herein.

In one embodiment of model construction 52, an operator of surface scanning controller 50 via input devices and/or graphical interfaces provides or selects a viscoelastic property parameter k as a constant value representative viscoelastic properties of the subject anatomical organ, and further provides or selects a scanning force parameter f_{DC} at which the surface of the anatomical organ will be scanned (e.g., a contact force in meganewtons). A surface deformation offset u_{SDO} is calculated from the provided/selected viscoelastic property parameter k and scanning force parameter f_{DC} to support the construction of the inoperative volume model 17 of the anatomical organ.

Alternatively, the present disclosure recognizes a viscoelastic behavior of a soft tissue of an anatomical organ under deformation may be a very complex process. First, the viscoelastic parameters for any unevenly distributed force may be described by a multi-dimensional matrix, which takes into account the direction of the force and topology of the surface. Second, a linearity of the deformation holds true only for very small deformations (e.g., in the order of nanometers). Third, a viscoelastic property parameters k of the soft tissue of the anatomical organ may be either unknown due to tissue abnormalities or due to patient-specific anatomical characteristics. Thus, in a

second embodiment of model construction 52, surface deformation offset u_{SDO} is empirically defined as will be further explained herein.

Still referring to FIGS. 1A and 1B, as surface scanning controller 50 controls a navigation of surgical scanning end-effector 43 relative to the anatomical organ in accordance with the planned sampling scan path delineated on preoperative image segmented volume model 15 of the anatomical organ, robotic surface scanning phase 12 of method 10 further encompasses surface scanning controller 50 recording each positon of the calibrated scanned reference of scanning surface end-effector 43 that correspond to a contact force applied by surface scanning end-effector 43 to the anatomical organ equaling scanning force parameter f_{DC} . In practice, the sensed contact form equaling the scanning force parameter f_{DC} may be enforced with an acceptable margin of error.

Each recorded positon of the calibrated scanned reference of scanning surface end-effector 43 is deemed a digitized model point suitable for a generation of a sparse point cloud representation of the anatomical organ on the assumption of a uniform deformation offset of each recorded position of a digitized model point.

In practice, as will be further explained herein, a line sampling scan path generates a sparse point cloud representation of the anatomical organ in view of a subset of positons of the calibrated scanned reference of scanning surface end-effector 43 corresponding to a contact force applied by surface scanning end-effector 43 to the anatomical organ equaling scanning force parameter f_{DC} and further in view a subset of positons of the calibrated scanned reference of scanning surface end-effector 43 failing to correspond to a contact force applied by surface scanning end-effector 43 to the anatomical organ equaling scanning force parameter f_{DC} .

Also in practice, as will be further explained herein, a point sampling scan path generates a sparse point cloud representation of the anatomical organ based on the spatial delineation of the points on preoperative image segmented volume model 15 of the anatomical organ.

For non-imaging embodiments of scanning surface end-effector 43, robotic surface scanning phase 12 of method 10 further encompasses surface scanning controller 50 constructing intraoperative volume model 17 as a mesh created from the

sparse point cloud representation via any mesh construction technique known in the art of the present disclosure (e.g. ,a Delaunay triangulation).

Due to the defined deformation offset, the mesh will have a comparable shape to a shape of the preoperative image segmented volume model 15 of the anatomical organ for registration purposes, but the mesh will have a not necessarily have a comparable size to a size of the preoperative image segmented volume model 15 of the anatomical organ. While not necessary for most registration processes, to achieve comparable sizes, surface scanning controller 50 may further calculate normal vectors at each vertex as a function of the defined deformation offset via any mesh normalization technique known in the art of the present disclosure (e.g. ,a Mean Weight Equal), and displace each point of the mesh in a direction of the associated normal vector to increase the size yet maintain the shape of the mesh.

For imaging embodiments of scanning surface end-effector 43, robotic surface scanning phase 12 of method 10 further encompasses surface scanning controller 50 stitching images associated with each point of the mesh, unsized or sized to thereby render intraoperative volume model 17 as an image of the anatomical organ. In practice, while stitching images associated with each point of the mesh, surface scanning controller 50 may interpolate images missing from the mesh due to unrecorded positions of the calibrated scanned reference of scanning surface end-effector 43.

To facilitate an understanding of the various inventions of the present disclosure, the following description of FIGS. 3A-3C illustrates exemplary recorded positions of digitize model points in accordance with the inventive principles of the present disclosure. From this description, those having ordinary skill in the art will further appreciate how to practice various and numerous embodiments of force sensed surface scanning methods and force sensed surface scanning systems in accordance with the inventive principles of the present disclosure. .

Referring to FIG. 3A, surface scanning end-effector 43 is shown deforming an anatomical organ prior to a scanning of the surface of the anatomical organ. More particularly, surface scanning controller 50 controls a positioning of scanning end-effector 43 relative to the anatomical organ to initially apply a contact force unto the tissue of the anatomical organ resulting in an OFFSET₁ between undeformed

anatomical tissue UAT and deformed anatomical tissue DAT_I. The positioning of scanning end-effector 43 is adjusted until a sensed contact force SCF_I per force sensing data FSD equals a desired contract force DCF whereby OFFSET_I between undeformed anatomical tissue UAT and deformed anatomical tissue DAT_I is deemed to equate the defined surface deformation offset u_{SDO} of the anatomical organ as previously described herein. Consequently, from a corresponding robot positon RP_I per robot position data 45, surface scanning controller 50 records calibrated scanned reference positon SRP of surface scanning end-effector 43 represented by the black dot as the initial digitized model point DMP_I.

During a scanning of the surface of the anatomical organ, FIG. 3A illustrates a repositioning of scanning end-effector 43 to a robot positon RP_X relative to the anatomical organ resulting in OFFSET_X between undeformed anatomical tissue UAT and deformed anatomical tissue DAT_X with a sensed contact force SCF_X per force sensing data FSD equals a desired contract force DCF, and FIG. 3B illustrates a repositioning of scanning end-effector 43 to a robot positon RP_Y relative to the anatomical organ resulting in OFFSET_Y between undeformed anatomical tissue UAT and deformed anatomical tissue DAT_Y with a sensed contact force SCF_Y per force sensing data FSD that does not equal a desired contract force DCF.

For point sampling scan path embodiments, the repositioning of scanning end-effector 43 is adjusted until a sensed contact force SCF per force sensing data FSD equals a desired contract force DCF as shown in FIG. 3A whereby OFFSET_X between undeformed anatomical tissue UAT and deformed anatomical tissue DAT_X is deemed to equate the defined surface deformation offset u_{SDO} of the anatomical organ as previously described herein. Consequently, from a corresponding robot positon RP_X per robot position data 45, surface scanning controller 50 records calibrated scanned reference positon SRP of surface scanning end-effector 43 represented by the black dot as an additional digitized model point DMP_X. This process is repeated for each point in the point sampling scan path.

For line sampling scan path embodiments, as surface sensing end-effector 43 is traversed along a line over the surface of the anatomical organ, surface scanning controller 50 will digitize robot positions RP_X as shown in FIG. 3A and will not digitize

robot positions RP_Y as shown in FIG. 3B or any other robot positon failing to sense a contact force equaling the scanning force parameter SFP.

The result for either embodiment is a spare cloud representation of the anatomical organ facilitating of an unsized or resized mesh creation of inoperative 5 volume model 17.

Referring back to FIGS. 1A and 1B, volume model registration 13 of method 10 encompasses surface scanning controller 50 implementing a model registration 53 of preoperative segmented volume model 15 and intraoperative volume model 17 via a registration technique as known in the art of the present disclosure.

10 In mesh embodiments of intraoperative volume model 17, surface scanning controller 50 may execute a point-by-point registration technique for registering preoperative segmented volume model 15 and intraoperative volume model 17. Examples of such a point-by-point registration technique include, but are not limited to, a rigid or non-rigid Iterative Closer Point (ICP) registration, a rigid or non-rigid Robust 15 Point Matching (RPM) registration and a particle filter based registrations.

In stitched image embodiments of intraoperative volume model 17, surface scanning controller 50 may execute an image registration technique for registering preoperative segmented volume model 15 and intraoperative volume model 17. Examples of such a point-by-point registration technique include, but are not limited to, 20 an internal anatomical landmark based image registration (e.g., bifurcations or calcifications), an internal implanted marker based image registration and a mutual information based image registration.

Still referring FIGS. 1A and 1B, upon completion of the scanning process, surface scanning controller 50 may implement a model fusion 54 based on model 25 registration 53 as known in the art of the present disclosure whereby a registered model fusion 56 may be displayed within an applicable coordinate system as symbolically shown.

In one embodiment, registered model fusion 56 includes an overlay of preoperative segmented volume model 15 onto intraoperative volume model 17.

30 In another embodiment, registered model fusion 56 includes an overlay of preoperative segmented volume model 15 onto the anatomical organ as registered to the a coordinate system of robotic system 40.

To facilitate an understanding of the various inventions of the present disclosure, the following description of FIGS. 4 and 5 teaches additional embodiments of a force sensed surface scanning system 100 and a force sensed surface scanning system 140 in accordance with the inventive principles of the present disclosure. From 5 this description, those having ordinary skill in the art will further appreciate how to practice various and numerous embodiments of force sensed surface scanning methods and force sensed surface scanning systems in accordance with the inventive principles of the present disclosure.

Referring to FIG. 4, force sensed surface scanning system 100 employs a snake 10 scanning robot 110, a tool pointer 113, an ultrasound laparoscope 115 and an endoscope 115.

For scanning purposes, tool pointer 113 or ultrasound laparoscope 115 may be mounted onto snake scanning robot 110 as known in the art of the present disclosure.

Snake scanning robot 110 is equipped with either force/pressure sensor(s) 111 15 and/or optical fiber(s) 112 for sensing a contact force applied by a mounted tool pointer 113 or ultrasound laparoscope 115 to an anatomical organ as known in the art of the pressure disclosure.

Endoscope 115 is mountable on additional snake scanning robot 110 for 20 purposes of viewing a positioning of tool pointer 113 or ultrasound laparoscope 115 in proximity of a surface of an anatomical organ.

Force sensed surface scanning system 100 further employs a workstation 120 and a scanning control device 130.

Workstation 120 includes a known arrangement of a monitor 121, a keyboard 122 and a computer 123 as known in the art of the present disclosure.

Scanning control device 130 employs a robot controller 131, a surface scanning controller 132 and a display controller 137, all installed on computer 123.

In practice, robot controller 131, surface scanning controller 132 and display controller 137 may embody any arrangement of hardware, software, firmware and/or electronic circuitry for implementing a force sensed surface scanning method as shown 30 in FIG. 5 in accordance with the inventive principles of the present disclosure as will be further explained herein.

In one embodiment, robot controller 131, surface scanning controller 132 and display controller 137 each may include a processor, a memory, a user interface, a network interface, and a storage interconnected via one or more system buses.

The processor may be any hardware device, as known in the art of the present disclosure or hereinafter conceived, capable of executing instructions stored in memory or storage or otherwise processing data. In a non-limiting example, the processor may include a microprocessor, field programmable gate array (FPGA), application-specific integrated circuit (ASIC), or other similar devices.

The memory may include various memories, as known in the art of the present disclosure or hereinafter conceived, including, but not limited to, L1, L2, or L3 cache or system memory. In a non-limiting example, the memory may include static random access memory (SRAM), dynamic RAM (DRAM), flash memory, read only memory (ROM), or other similar memory devices.

The user interface may include one or more devices, as known in the art of the present disclosure or hereinafter conceived, for enabling communication with a user such as an administrator. In a non-limiting example, the user interface may include a command line interface or graphical user interface that may be presented to a remote terminal via the network interface.

The network interface may include one or more devices, as known in the art of the present disclosure or hereinafter conceived, for enabling communication with other hardware devices. In a non-limiting example, the network interface may include a network interface card (NIC) configured to communicate according to the Ethernet protocol. Additionally, the network interface may implement a TCP/IP stack for communication according to the TCP/IP protocols. Various alternative or additional hardware or configurations for the network interface will be apparent.

The storage may include one or more machine-readable storage media, as known in the art of the present disclosure or hereinafter conceived, including, but not limited to, read-only memory (ROM), random-access memory (RAM), magnetic disk storage media, optical storage media, flash-memory devices, or similar storage media. In various non-limiting embodiments, the storage may store instructions for execution by the processor or data upon which the processor may operate. For example, the storage may store a base operating system for controlling various basic operations of the

hardware. The storage may further store one or more application modules in the form of executable software/firmware.

More particularly, still referring to FIG. 4, robot controller 131 includes application module(s) for controlling a navigation of snake scanning robot 100 within a robotic coordinate system as known in the art of the present disclosure, and display controller 137 includes application module(s) for controlling an display of images, graphical user interfaces, etc. on monitor 120 as known in the art of the present disclosure.

Surface scanning controller 132 includes application modules in the form of a scanning commander (133) 133, a model constructor (134) 134, a model registor 135 and a model fuser 136 for controlling the implementation of the force sensed surface scanning method as shown in FIG. 5 in accordance with the inventive principles of the present disclosure as will be further explained herein.

In practice, scanning control device 130 may be alternatively or concurrently installed on other types of processing devices including, but not limited to, a tablet or a server accessible by workstations and tablets, or may be distributed across a network supporting an execution of a surgical procedure utilizing a force sensed surface scanning method of the present disclosure as shown in FIG. 5.

Also in practice, controllers 131, 132 and 135 may be integrated components, segregated components or logically partitioned components of scanning control device 130.

FIG. 5 illustrates a flowchart 140 representative of a force sensed surface scanning method in accordance with the inventive principles of the present disclosure that is implemented by application modules 133-136 of surface scanning controller 132 as will now be described herein.

Referring to FIG. 5, a stage S142 of flowchart 140 encompasses pre-scanning activities implemented by scanning commander (133) 132 (FIG. 4). These pre-scanning activities include, but are not limited to,

30 1. scanning commander 133 controlling a registration of snake scanning robot 110 and a preoperative segmented volume model registration as known in the art;

2. scanning commander 133 controlling a planning of a sampling scanning path for snake scanning robot 110 as previously described herein in connection with the description of FIGS. 1A and 1B, 5 particularly a line sampling scanning path or a point sampling scanning path;
3. scanning commander 133 controlling a graphical user interface for an operator provision or an operator selection of viscoelastic 10 property parameter k and scanning force parameter f ; and
4. scanning commander 133 controlling an initial offset positioning of a surface sensing end-effector, such as, for example, an initial 15 positioning of tool pointer 113 as shown in FIG. 6A or an initial positioning of ultrasound laparoscope 114 as shown in FIG. 7A.

More particularly, a defined surface deformation offset u is calculated from the provided/selected viscoelastic property parameter k and scanning force parameter f whereby scanning parameter 133 controls the initial offset positioning of the surface sensing end-effector to equate a sensed contact force to scanning force parameter f to thereby achieve a defined surface deformation offset u between an undeformed anatomical tissue and a deformed anatomical tissue of the anatomical organ as previously described herein. 20

For embodiments whereby viscoelastic property parameter k is known, defined surface deformation offset u may be empirically defined by:

25

1. scanning commander 133 controlling a graphical user interface for operator control of an initial offset positioning of a surface sensing end-effector at a selected non-zero sensed control force, such as, for example, an initial positioning of tool pointer 113 as shown in FIG. 6A or an initial positioning of ultrasound laparoscope 114 as shown in FIG. 30 7A; and

2. scanning commander 133 retracting the surface sensing end-effector until such time the sensed control force is zero; and
3. scanning commander 133 defining scanned force parameter f as the selected non-zero sensed control force associated with the initial offset positioning of the surface sensing end-effector, and further defining surface deformation offset u as the retraction distance of the surface sensing end-effector.

10 Alternatively in practice, a sampling scan path may be defined independent of the preoperative image segmented volume during stage S142, thereby omitting a requirement to register snake scanning robot 110 to the preoperative segmented volume model. For example, the sampling scan path may be defined as a geometric pattern (e.g., a spiral pattern, a zigzag pattern, etc.) or as a random pattern (e.g., a white noise sampling scheme) or a combination thereof. For such alternatively embodiment of stage S142, a surface of the anatomical organ is exposed via a surgical port, and the snake scanning robot 110 is inserted through the surgical port to the surface of the anatomical organ until reaching the initial offset positioning of the surface sensing end-effector or a position for an empirical definition of the surface deformation offset u .

15 Thereafter snake scanning robot 110 is manually or controller operated to follow a predefined geometric pattern or to randomly traverse the surface of the anatomical organ or a combination thereof.

20

Still referring to FIG. 5, a stage S144 of flowchart 140 encompasses scanning activities implemented by scanning commander (133) 132 (FIG. 4) and model constructor (134) 134 (FIG. 4). These scanning activities include, but are not limited to,

1. scanning commander 133 controlling a navigation of snake scanning robot 110 relative to the anatomical organ in accordance with the planned sampling scan path as previously described herein in connection with the description of FIGS. 1A and 1B; and

2A. model constructor 134 constructing an intraoperative volume mesh as previously described herein in connection with the description of FIGS. 1A and 1B, such as for example, an intraoperative volume mesh 170 shown in FIG. 6E; or

5

2B. model constructor 134 stitching an intraoperative volume image as previously described herein in connection with the description of FIGS. 1A and 1B, such as for example, an intraoperative volume image 180 shown in FIG. 7E.

10

More particular to embodiments of stage S144 utilizing tool pointer 113, the navigation of snake scanning robot 110 will result in a digitization of sample points indicating a sensed contact force equating scanned force parameter f as exemplary shown in FIG. 6B and a non-digitization of sample point indicating a sensed contact force not equating scanned force parameter f as exemplary shown in FIG. 6C.

15

Referring to FIG. 6D, a graph 150 may be displayed to an operator of workstation 120 (FIG. 4) to thereby visualize digitization time periods 152 and 154 of specific sample point(s) and non-digitization time periods 151, 153 and 155 of the remaining sample point(s).

20

In one embodiment, non-digitization time period 151 represents a pre-scanning positioning of tool pointer 113 relative to the anatomical region with digitization time periods 152 and 154 representing multiple digitized sample points during a line sampling scan of the anatomical organ.

25

In another embodiment, non-digitization 151 time period represents a pre-scanning positioning of tool pointer 113 relative to the anatomical region with digitization time periods 152 and 154 representing a single digitized sample point during a point sampling scan of the anatomical organ.

30

Referring back to FIG. 4, more particular to embodiments of stage S144 utilizing ultrasound laparoscope 114, the navigation of snake scanning robot 110 will result in a digitization of sample points indicating a sensed contact force equating scanned force parameter f as exemplary shown in FIG. 7B and a non-digitization of

sample point indicating a sensed contact force not equating scanned force parameter f as exemplary shown in FIG. 7C.

Referring to FIG. 7D, a graph 170 may be displayed to an operator of workstation 120 (FIG. 4) to thereby visualize digitization time periods 172 and 174 of specific sample point(s) and non-digitization time periods 171, 173 and 175 of the remaining sample point(s).

In one embodiment, non-digitization time period 171 represents a pre-scanning positioning of ultrasound laparoscope 114 relative to the anatomical region with digitization time periods 172 and 174 representing multiple digitized sample points during a line sampling scan of the anatomical organ.

In another embodiment, non-digitization 151 time period represents a pre-scanning positioning of ultrasound laparoscope 114 relative to the anatomical region with digitization time periods 172 and 174 representing a single digitize sample point during a point sampling scan of the anatomical organ.

Referring back to FIG. 4, a stage S146 of flowchart 140 encompasses post-scanning activities implemented by model constructor (134) 134 (FIG. 4) and/or model register 135. These post-scanning activities include, but are not limited to,

1A. model constructor 134 optionally controlling resizing of the intraoperative volume mesh as a function of the defined surface deformation offset as previously described herein in connection with the description of FIGS. 1A and 1B, such as, for example, a resizing of an intraoperative volume mesh 150 to an intraoperative volume mesh 151 as shown in FIG. 6F (note the resizing will normally be in nanometers, thus the resizing as shown in FIG. 6F is exaggerated to visualize the concept); and

2A. model register 135 registering the unsized/resized intraoperative volume mesh to the preoperative segmented volume model as previously described herein in connection with the description of FIGS. 1A and 1B; or

1B. model constructor 134 optionally controlling resizing of the intraoperative volume image as a function of the defined surface deformation offset as previously described herein in connection with the description of FIGS. 1A and 1B, such as, for example, a resizing of an intraoperative volume image 180 to an intraoperative volume mesh 181 as shown in FIG. 7F (note the resizing will normally be in nanometers, thus the resizing as shown in FIG. 7F is exaggerated to visualize the concept); and

10 2B. model register 135 registering the unsized/resized intraoperative volume image to the preoperative segmented volume model as previously described herein in connection with the description of FIGS. 1A and 1B.

15 Upon completion of stage S146, model fuser 136 implements a fusion technique as known in the art of the present disclosure for generating a registered model fusion 138 as previously described herein whereby display controller 137 controls a display of registered model fusion 138 as shown.

Referring to FIGS. 1-7, those having ordinary skill in the art will appreciate numerous benefits of the present disclosure including, but not limited to, an improvement over surface scanning systems, devices, controllers and methods by the inventions of the present disclosure providing a construction of an intraoperative scanned volume model of an anatomical organ based upon a sensing of a contact force applied by a surface scanning end-effector of a scanning robot to the anatomical organ whereby the contact force is indicative of a defined surface deformation offset of the anatomical organ, thereby enhancing a registration of the intraoperative surface scanned volume model of the anatomical organ with a preoperative image segmented volume model of the anatomical organ.

Furthermore, as one having ordinary skill in the art will appreciate in view of the teachings provided herein, features, elements, components, etc. described in the present disclosure/specification and/or depicted in the Figures may be implemented in various combinations of electronic components/circuitry, hardware, executable

software and executable firmware and provide functions which may be combined in a single element or multiple elements. For example, the functions of the various features, elements, components, etc. shown/illustrated/depicted in the Figures can be provided through the use of dedicated hardware as well as hardware capable of executing

5 software in association with appropriate software. When provided by a processor, the functions can be provided by a single dedicated processor, by a single shared processor, or by a plurality of individual processors, some of which can be shared and/or multiplexed. Moreover, explicit use of the term “processor” should not be construed to refer exclusively to hardware capable of executing software, and can implicitly include, 10 without limitation, digital signal processor (“DSP”) hardware, memory (e.g., read only memory (“ROM”) for storing software, random access memory (“RAM”), non-volatile storage, etc.) and virtually any means and/or machine (including hardware, software, firmware, circuitry, combinations thereof, etc.) which is capable of (and/or configurable) to perform and/or control a process.

15 Moreover, all statements herein reciting principles, aspects, and embodiments of the invention, as well as specific examples thereof, are intended to encompass both structural and functional equivalents thereof. Additionally, it is intended that such equivalents include both currently known equivalents as well as equivalents developed in the future (e.g., any elements developed that can perform the same or substantially 20 similar function, regardless of structure). Thus, for example, it will be appreciated by one having ordinary skill in the art in view of the teachings provided herein that any block diagrams presented herein can represent conceptual views of illustrative system components and/or circuitry embodying the principles of the invention. Similarly, one having ordinary skill in the art should appreciate in view of the teachings provided 25 herein that any flow charts, flow diagrams and the like can represent various processes which can be substantially represented in computer readable storage media and so executed by a computer, processor or other device with processing capabilities, whether or not such computer or processor is explicitly shown.

Furthermore, exemplary embodiments of the present disclosure can take the 30 form of a computer program product or application module accessible from a computer-readable and/or computer-readable storage medium providing program code and/or instructions for use by or in connection with, e.g., a computer or any instruction

execution system. In accordance with the present disclosure, a computer-usable or computer readable storage medium can be any apparatus that can, e.g., include, store, communicate, propagate or transport the program for use by or in connection with the instruction execution system, apparatus or device. Such exemplary medium can be,

5 e.g., an electronic, magnetic, optical, electromagnetic, infrared or semiconductor system (or apparatus or device) or a propagation medium. Examples of a computer-readable medium include, e.g., a semiconductor or solid state memory, magnetic tape, a removable computer diskette, a random access memory (RAM), a read-only memory (ROM), flash (drive), a rigid magnetic disk and an optical disk. Current examples of
10 optical disks include compact disk – read only memory (CD-ROM), compact disk – read/write (CD-R/W) and DVD. Further, it should be understood that any new computer-readable medium which may hereafter be developed should also be considered as computer-readable medium as may be used or referred to in accordance with exemplary embodiments of the present disclosure and disclosure.

15 Having described preferred and exemplary embodiments of novel and inventive force sensed surface scanning systems, devices, controllers and methods, (which embodiments are intended to be illustrative and not limiting), it is noted that modifications and variations can be made by persons having ordinary skill in the art in light of the teachings provided herein, including the Figures. It is therefore to be
20 understood that changes can be made in/to the preferred and exemplary embodiments of the present disclosure which are within the scope of the embodiments disclosed herein.

Moreover, it is contemplated that corresponding and/or related systems incorporating and/or implementing the device or such as may be used/implemented in a
25 device in accordance with the present disclosure are also contemplated and considered to be within the scope of the present disclosure. Further, corresponding and/or related method for manufacturing and/or using a device and/or system in accordance with the present disclosure are also contemplated and considered to be within the scope of the present disclosure.

Claims

1. A force sensed surface scanning system (20), comprising:
a scanning robot (41) including a surface scanning end-effector (43) structurally
5 configured to generate force sensing data informative of a contact force applied by the
surface scanning end-effector (43) to an anatomical organ; and

10 a surface scanning controller (50) structurally configured to control a surface
scanning of the anatomical organ by the surface scanning end-effector (43) including
the surface scanning end-effector (43) generating the force sensing data,

15 wherein the surface scanning controller (50) is further structurally
configured to construct an intraoperative volume model of the anatomical organ
responsive to the force sensing data generated by the surface scanning end-effector (43)
indicating a defined surface deformation offset of the anatomical organ.

20 2. The force sensed surface scanning system (20) of claim 1,
wherein the intraoperative volume model is one of an intraoperative volume
mesh and an intraoperative volume image.

25 3. The force sensed surface scanning system (20) of claim 1,
wherein the surface scanning controller (50) is further structurally configured to
control an operator definition of the surface deformation offset as a function of a
viscoelastic property parameter and a scanned force parameter;

wherein the viscoelastic property parameter quantifies a stiffness of the
anatomical organ; and

30 4. The force sensed surface scanning system (20) of claim 1,
wherein the scanned force parameter quantifies a desired contact force for
digitizing surface points of the anatomical organ.

4. The force sensed surface scanning system (20) of claim 1,
wherein the surface scanning controller (50) is further structurally configured to
control an empirical definition of the surface deformation offset responsive to the force
sensing data generated by the surface scanning end-effector (43) indicating an operator

desired contact force applied by the surface scanning end-effector (43) to the anatomical organ.

5. The force sensed surface scanning system (20) of claim 1, wherein the surface scanning controller (50) is further structurally configured to at least one of:

define a sampling scan path traversing a preoperative segmented volume model of the anatomical organ; and

define a sampling scan path having at least one of a geometric pattern and a random pattern traversing the surface of the anatomical organ.

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6. The force sensed surface scanning system (20) of claim 1,

wherein the sampling scan path includes at least one of a line sampling scan path and a point sampling scan path.

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7. The force sensed surface scanning system (20) of claim 1,

wherein the surface scanning controller (50) is further structurally configured to control a resizing of a constructed intraoperative volume model of the anatomical organ as a function of the defined surface deformation offset of the anatomical organ.

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8. The force sensed surface scanning system (20) of claim 1,

wherein the surface scanning controller (50) is further structurally configured to control a registration of the intraoperative volume model of the anatomical organ and a preoperative segmented volume model of the anatomical organ.

25

9. The force sensed surface scanning system (20) of claim 1,

wherein the scanning robot (41) is a snake scanning robot (41).

10. The force sensed surface scanning system (20) of claim 1,

wherein the surface scanning end-effector (43) is one of a tool pointer and an

30

ultrasound laparoscope.

11. A surface scanning controller (50) for a scanning robot (41) including a surface scanning end-effector (43), the surface scanning controller (50) comprising:

5 a scanning commander (133) structurally configured to control a surface scanning of the anatomical organ by the surface scanning end-effector (43) including the surface scanning end-effector (43) generating force sensing data informative of a contact force applied by the surface scanning end-effector (43) to the anatomical organ; and

10 a model constructor (134) structurally configured to construct an intraoperative volume model of the anatomical organ responsive to the force sensing data generated by the surface scanning end-effector (43) indicating a defined surface deformation offset of the anatomical organ.

12. The surface scanning controller (50) of claim 11,

15 wherein the model constructor (134) is further structurally configured to control a definition of the surface deformation offset as a function of a viscoelastic property parameter and a scanned force parameter,

wherein the viscoelastic property parameter quantifies a stiffness of the anatomical organ, and

20 wherein the scanned force parameter quantifies a desired contact force for digitizing surface points of the anatomical organ.

13. The surface scanning controller (50) of claim 11,

the surface scanning controller (50) wherein the model constructor (134) is further structurally configured to control a definition of the surface deformation offset responsive to the force sensing data generated by the surface scanning end-effector (43) indicating an operator desired contact force applied by the surface scanning end-effector (43) to the anatomical organ.

14. The surface scanning controller (50) of claim 11, wherein the surface scanning commander (133) is further structurally configured to at least one of:

30 define a sampling scan path traversing a preoperative segmented volume model of the anatomical organ; and

define a sampling scan path having at least one of a geometric pattern and a random pattern traversing the surface of the anatomical organ.

15. The surface scanning controller (50) of claim 11,

5 wherein the model constructor (134) is further structurally configured to control a resizing a constructed intraoperative volume model of the anatomical organ as a function of the defined surface deformation offset of the anatomical organ.

16. A force sensed surface scanning method for a scanning robot (41) including a

10 surface scanning end-effector (43), the force sensed surface scanning method comprising:

15 a surface scanning controller (50) controlling a surface scanning of an anatomical organ by the surface scanning end-effector (43) scanning end-effector (43) including the surface scanning end-effector (43) generating force sensing data informative of a contact force applied by the surface scanning end-effector (43) to the anatomical organ; and

20 the surface scanning controller (50) constructing an intraoperative volume model of the anatomical organ responsive to the force sensing data generated by the surface scanning end-effector (43) indicating a defined surface deformation offset of the anatomical organ.

17. The force sensed surface scanning method of claim 16, further comprising:

the surface scanning controller (50) defining the surface deformation offset as a function of a viscoelastic property parameter and a scanned force parameter,

25 wherein the viscoelastic property parameter quantifies a stiffness of the anatomical organ, and

wherein the scanned force parameter quantifies a desired contact force for digitizing surface points of the anatomical organ.

30 18. The force sensed surface scanning method of claim 16, further comprising:

the surface scanning controller (50) defining the surface deformation offset responsive to the force sensing data generated by the surface scanning end-effector (43)

indicating an operator desired contact force applied by the surface scanning end-effector (43) to the anatomical organ.

19. The force sensed surface scanning method of claim 16, further comprising:

5 the surface scanning controller (50) delineating a sampling scan path on a preoperative segmented volume model of the anatomical organ.

20. The force sensed surface scanning method of claim 16, further comprising:

the surface scanning controller (50) resizing a constructed intraoperative 10 volume model of the anatomical organ as a function of the defined surface deformation offset of the anatomical organ.

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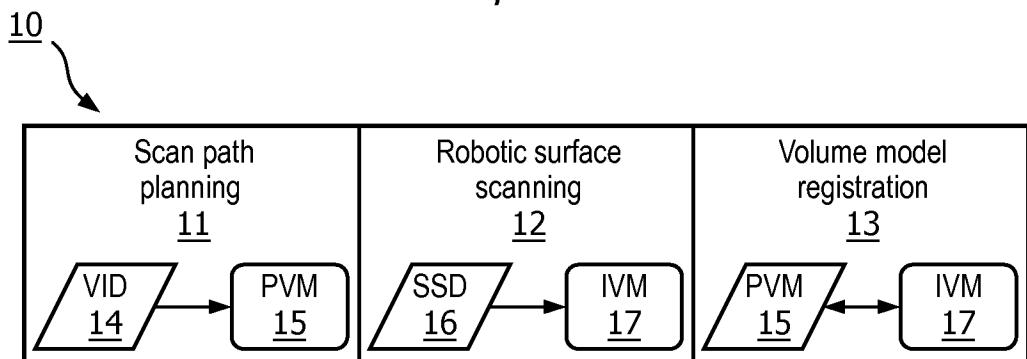


FIG. 1A

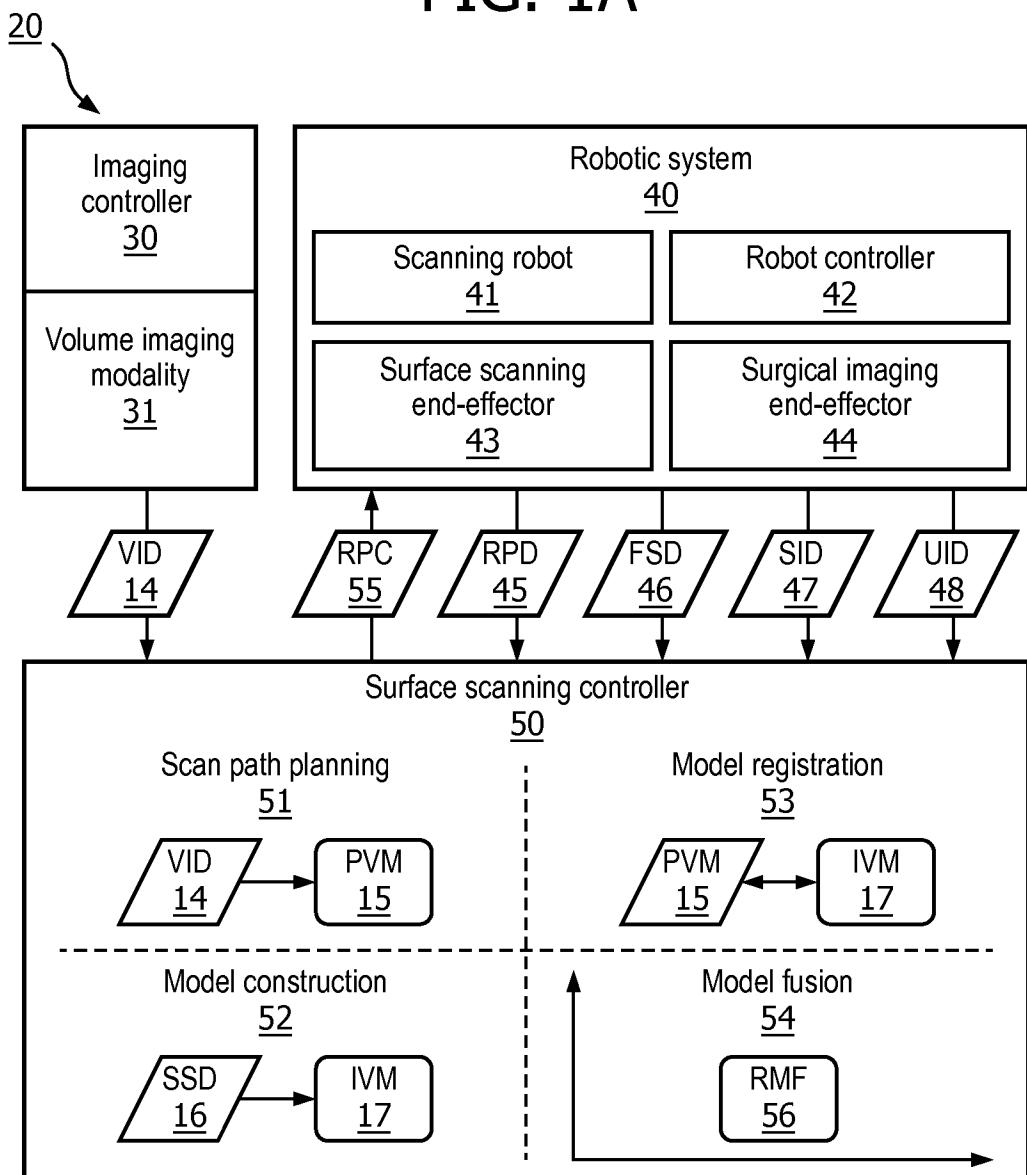


FIG. 1B

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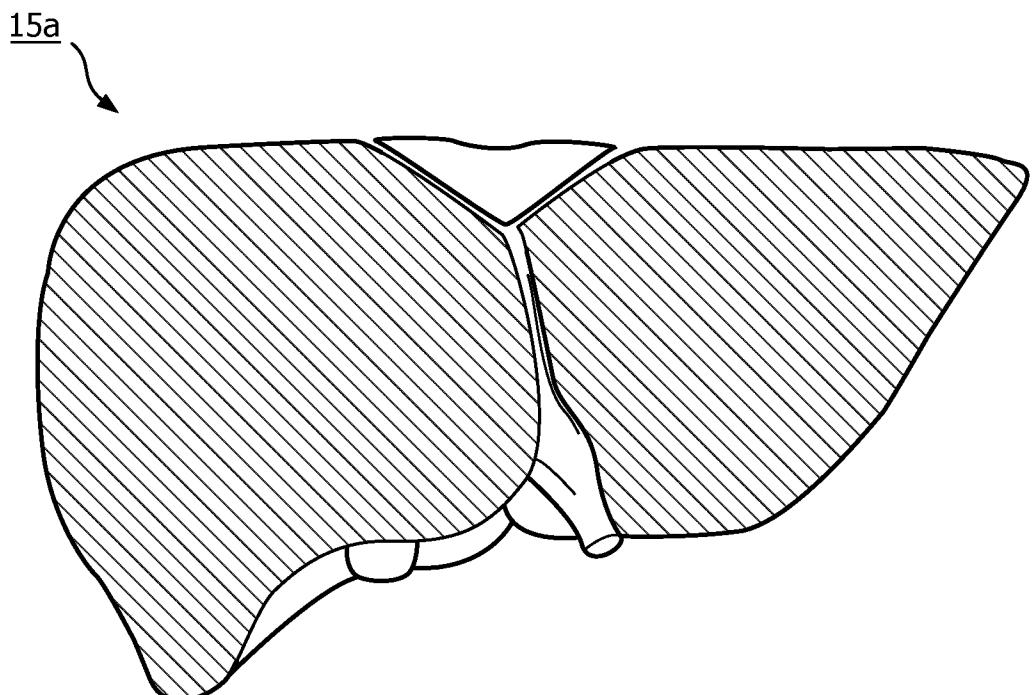


FIG. 2A

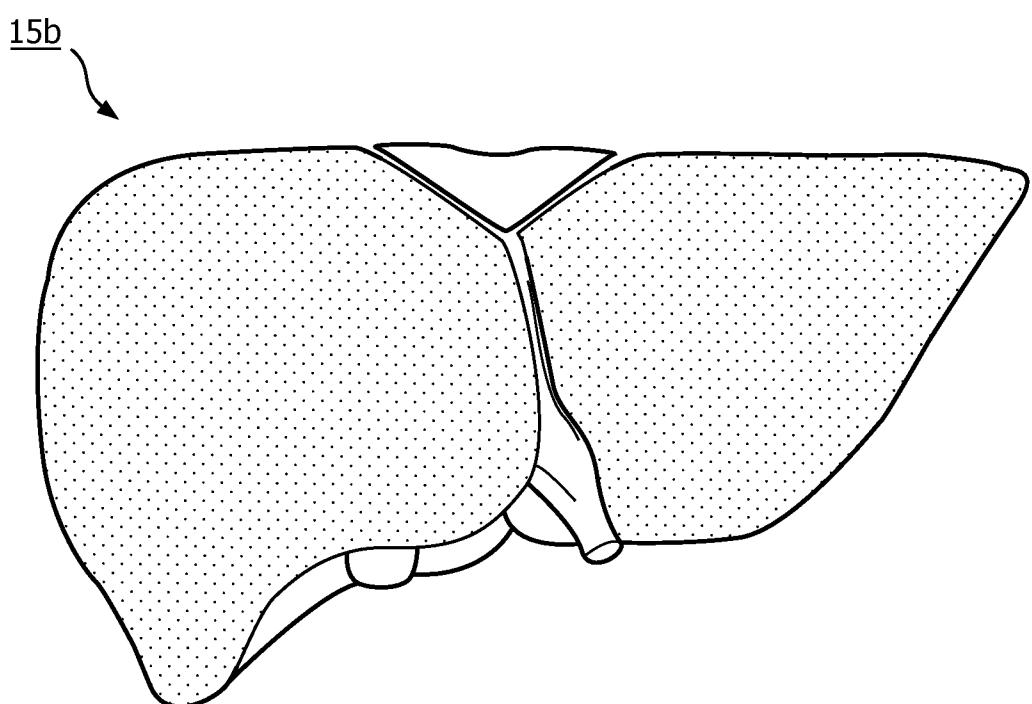


FIG. 2b

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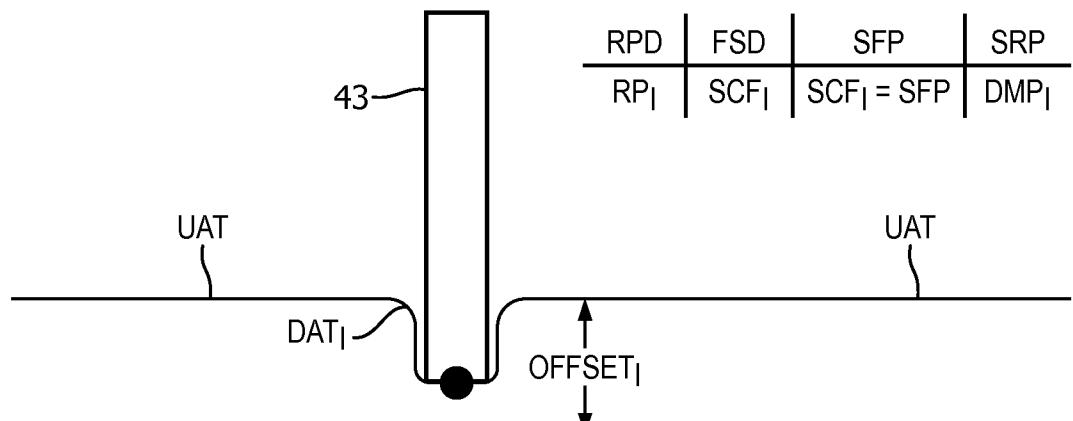


FIG. 3A

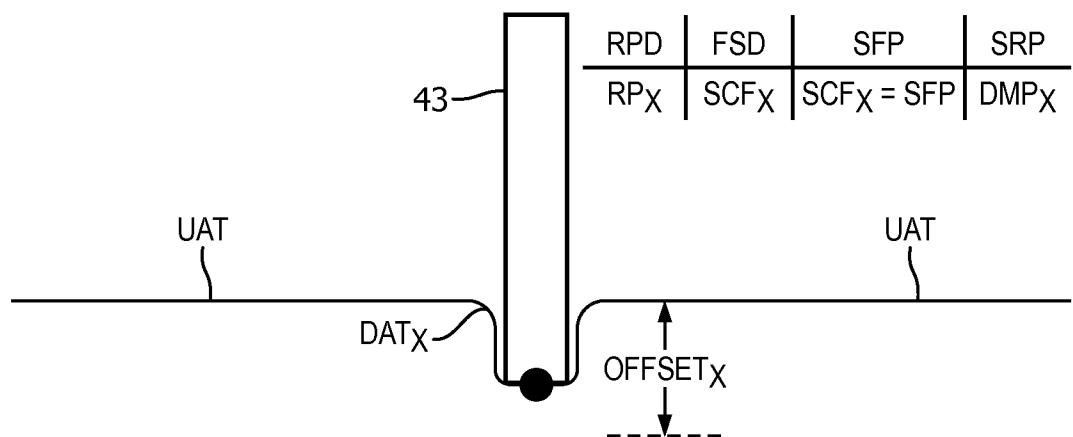


FIG. 3B

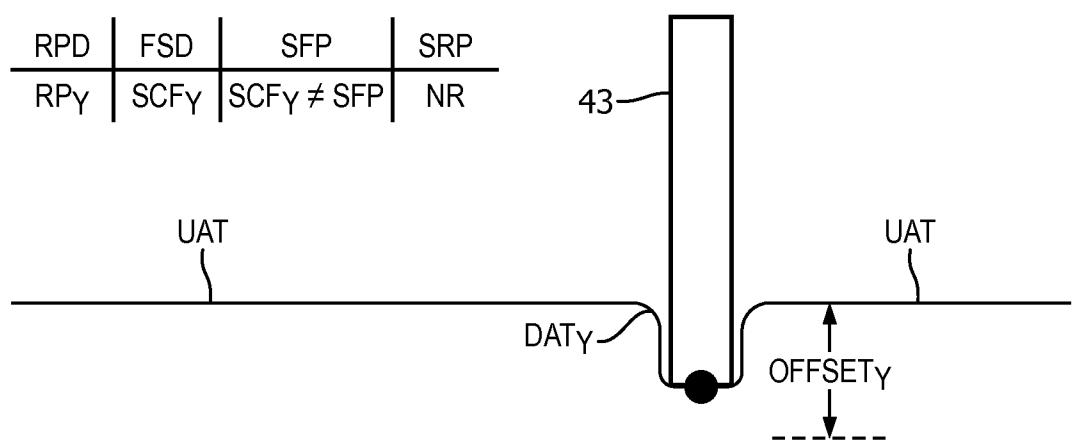


FIG. 3C

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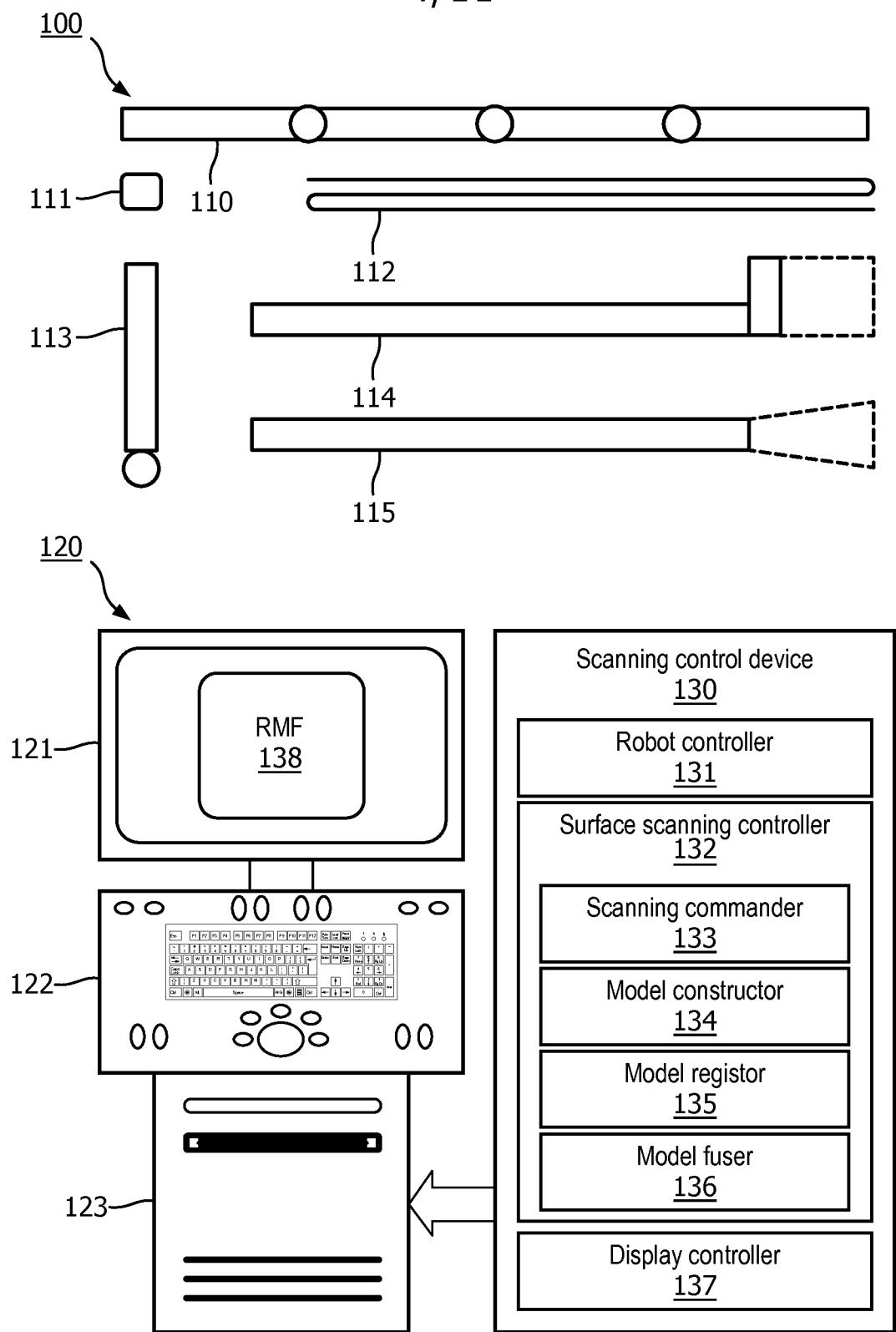


FIG. 4

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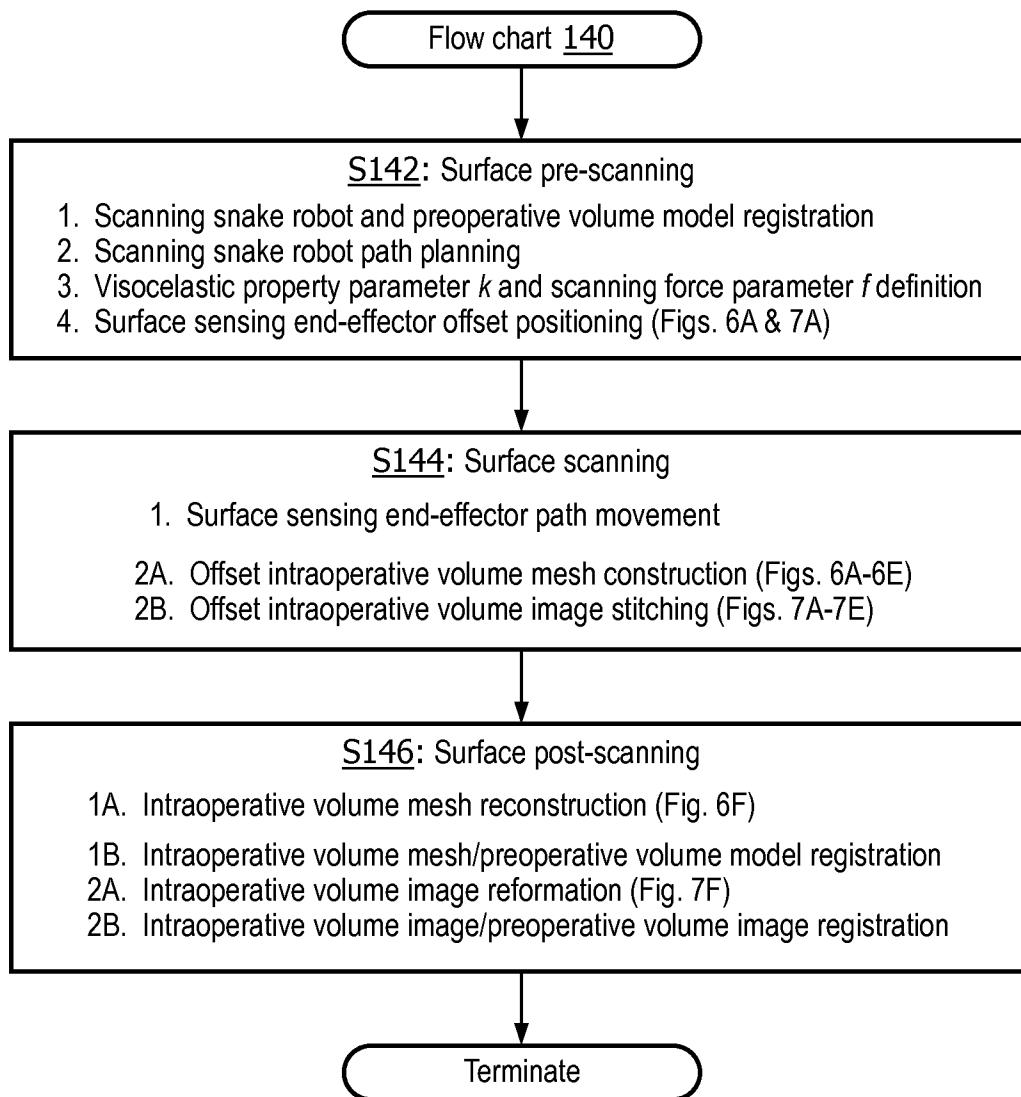


FIG. 5

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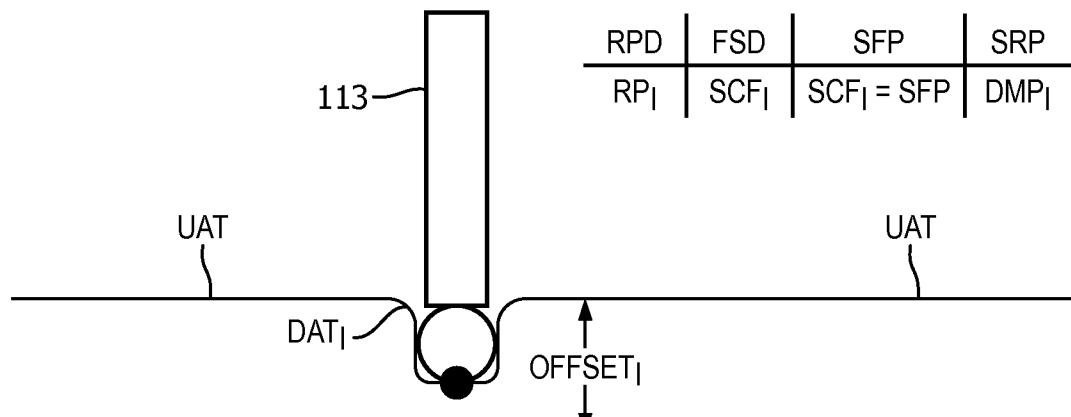


FIG. 6A

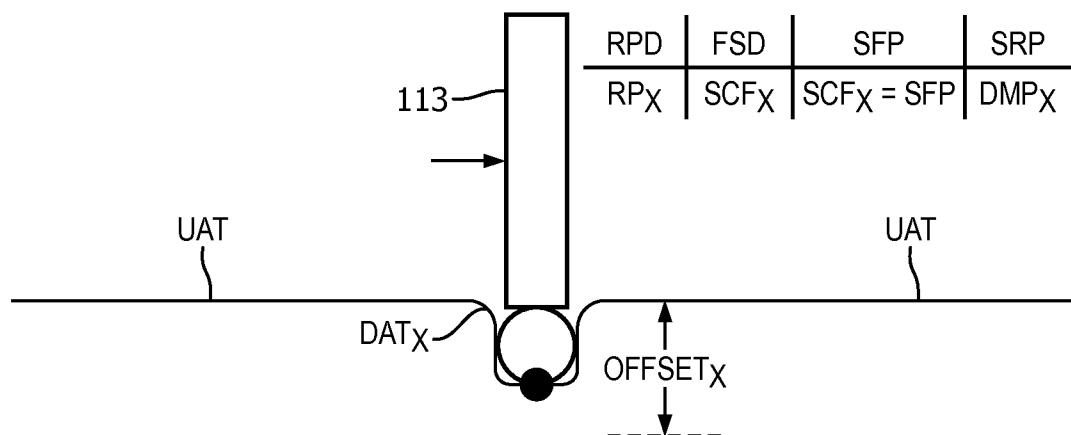


FIG. 6B

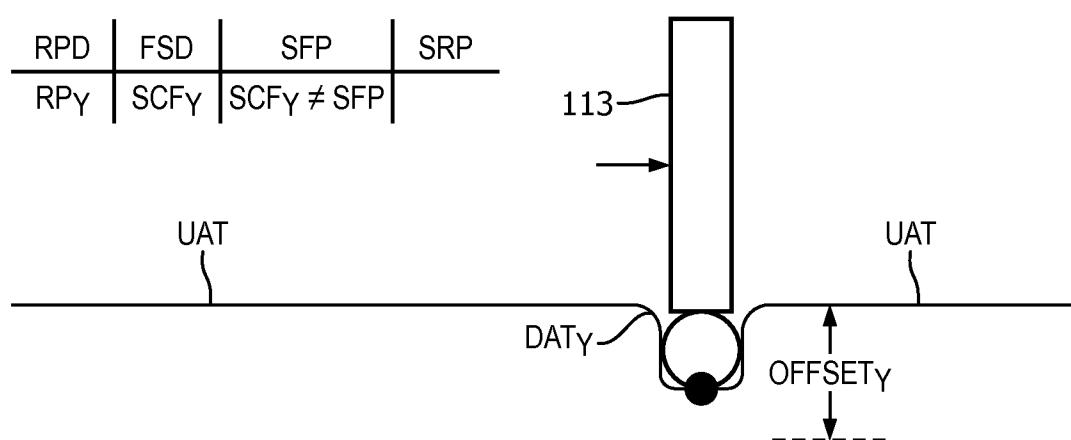


FIG. 6C

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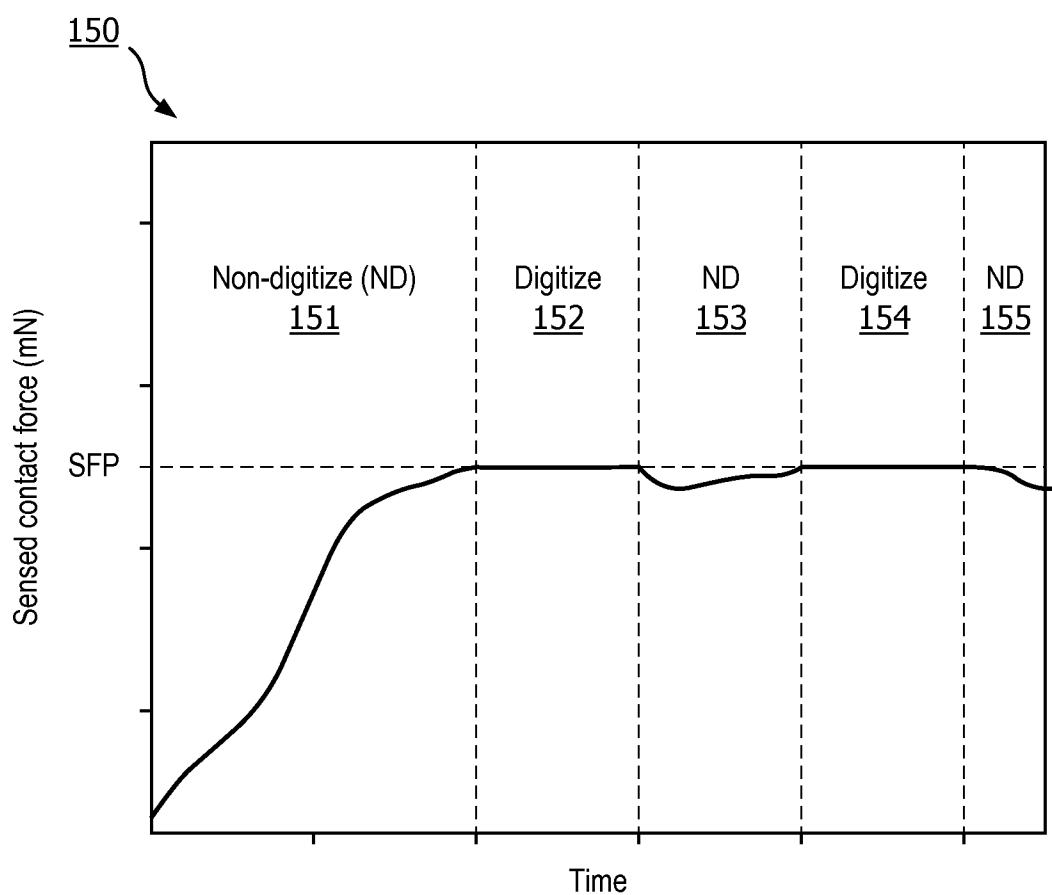


FIG. 6D

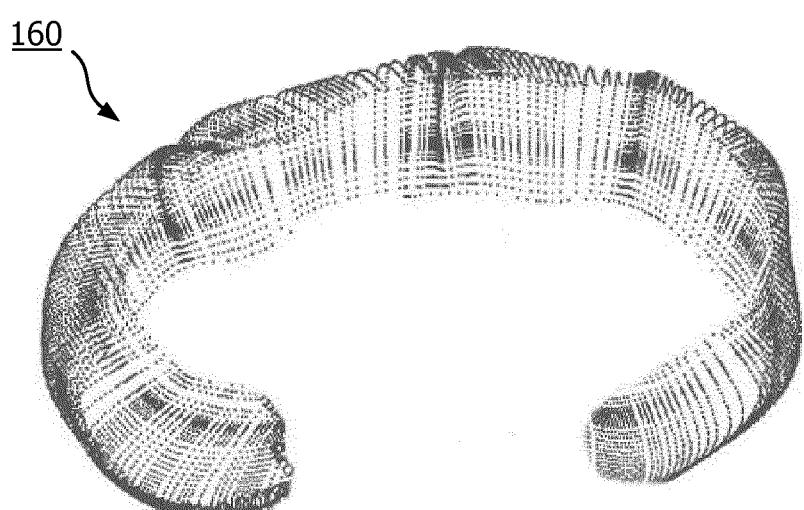


FIG. 6E

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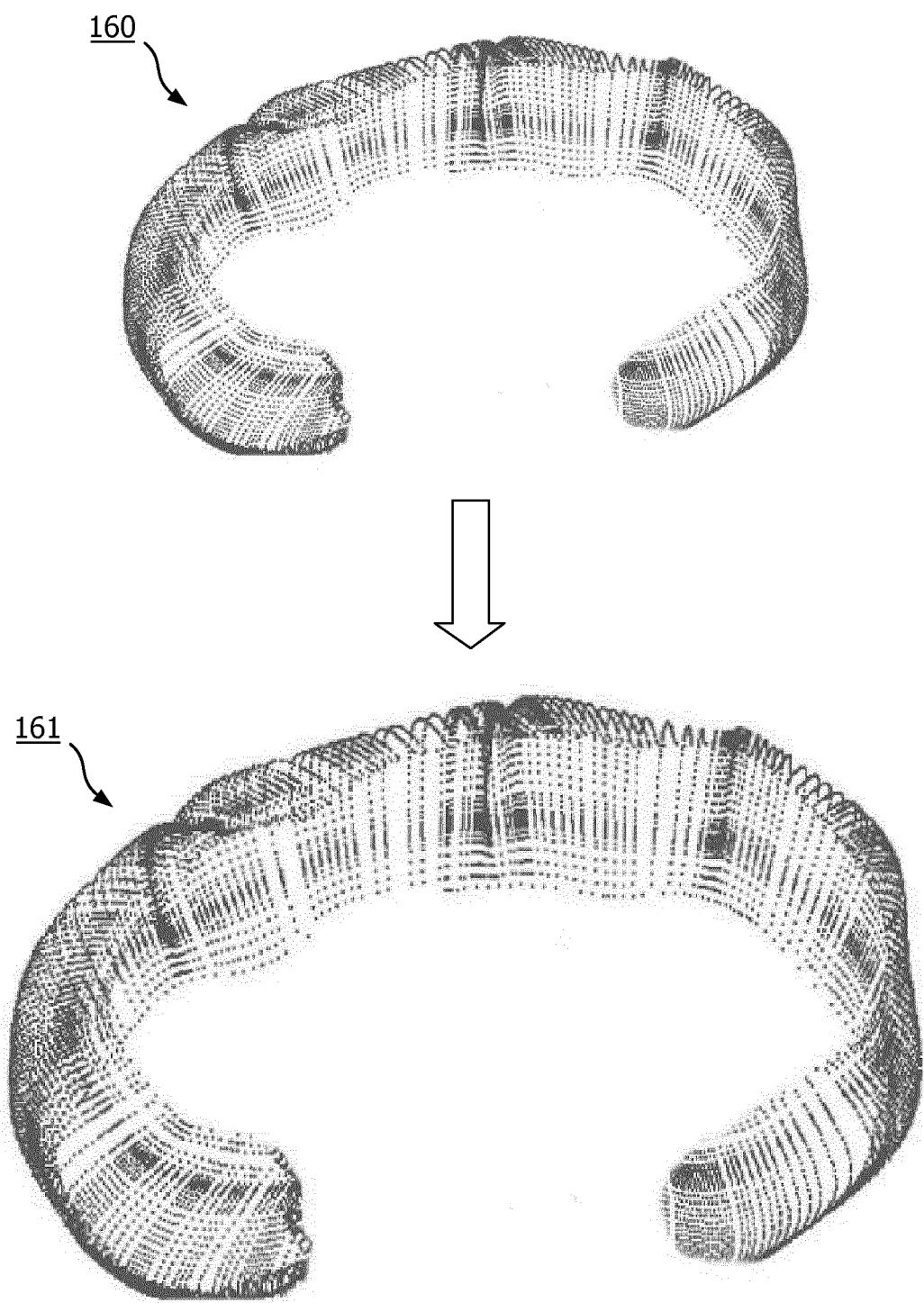


FIG. 6F

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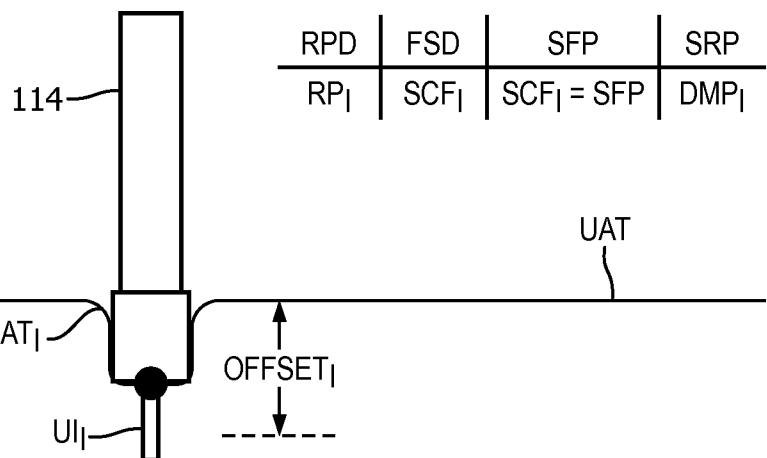


FIG. 7A

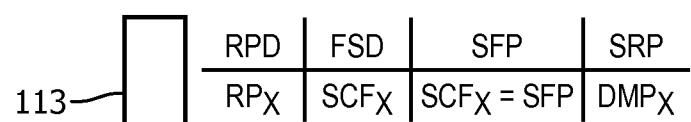


FIG. 7B

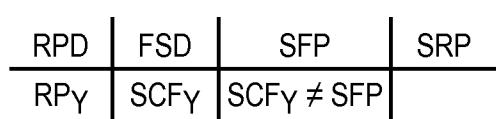


FIG. 7C

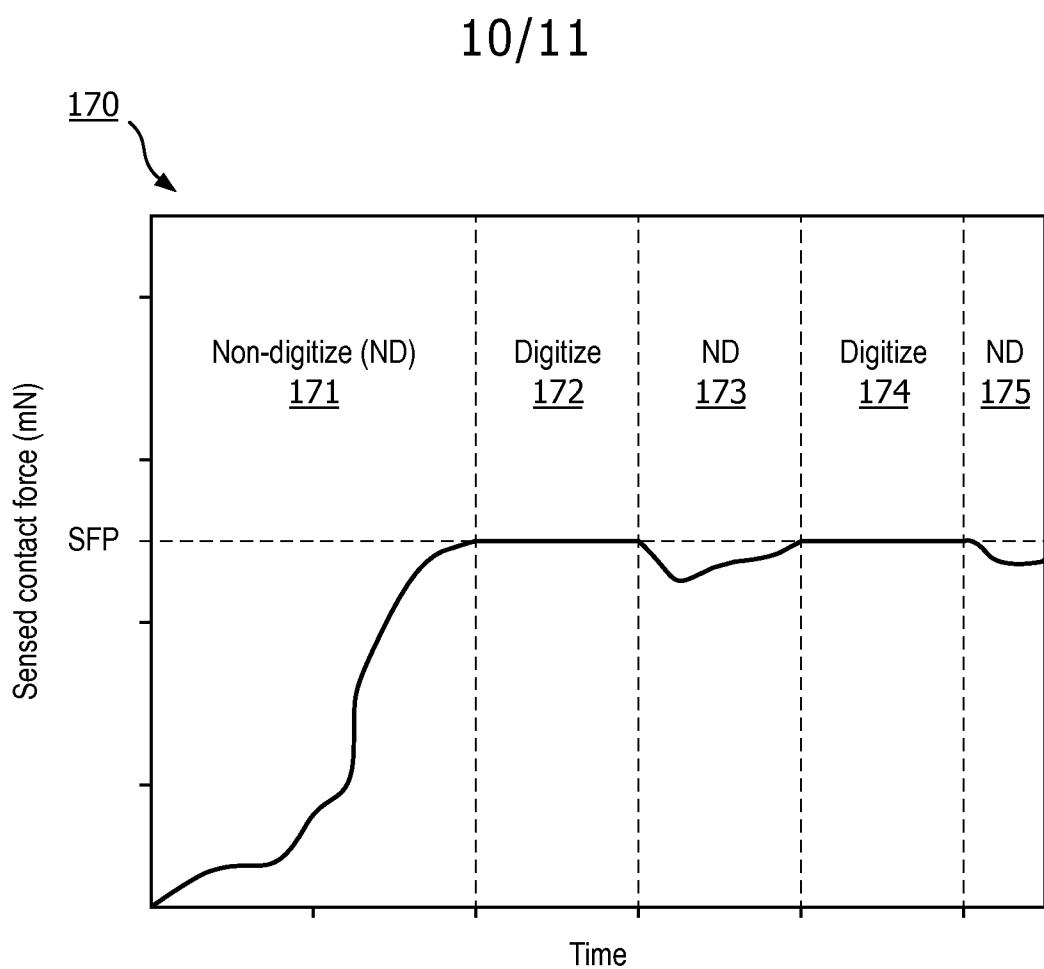


FIG. 7D

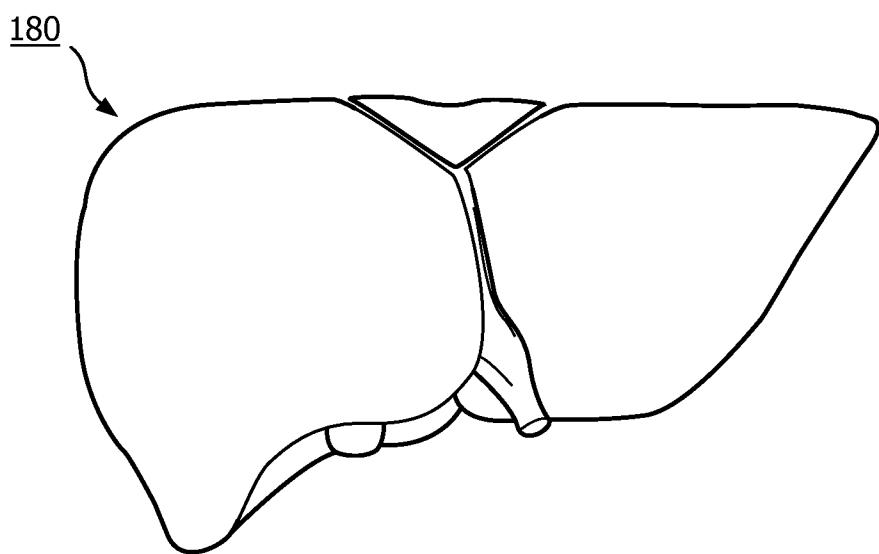


FIG. 7E

11/11

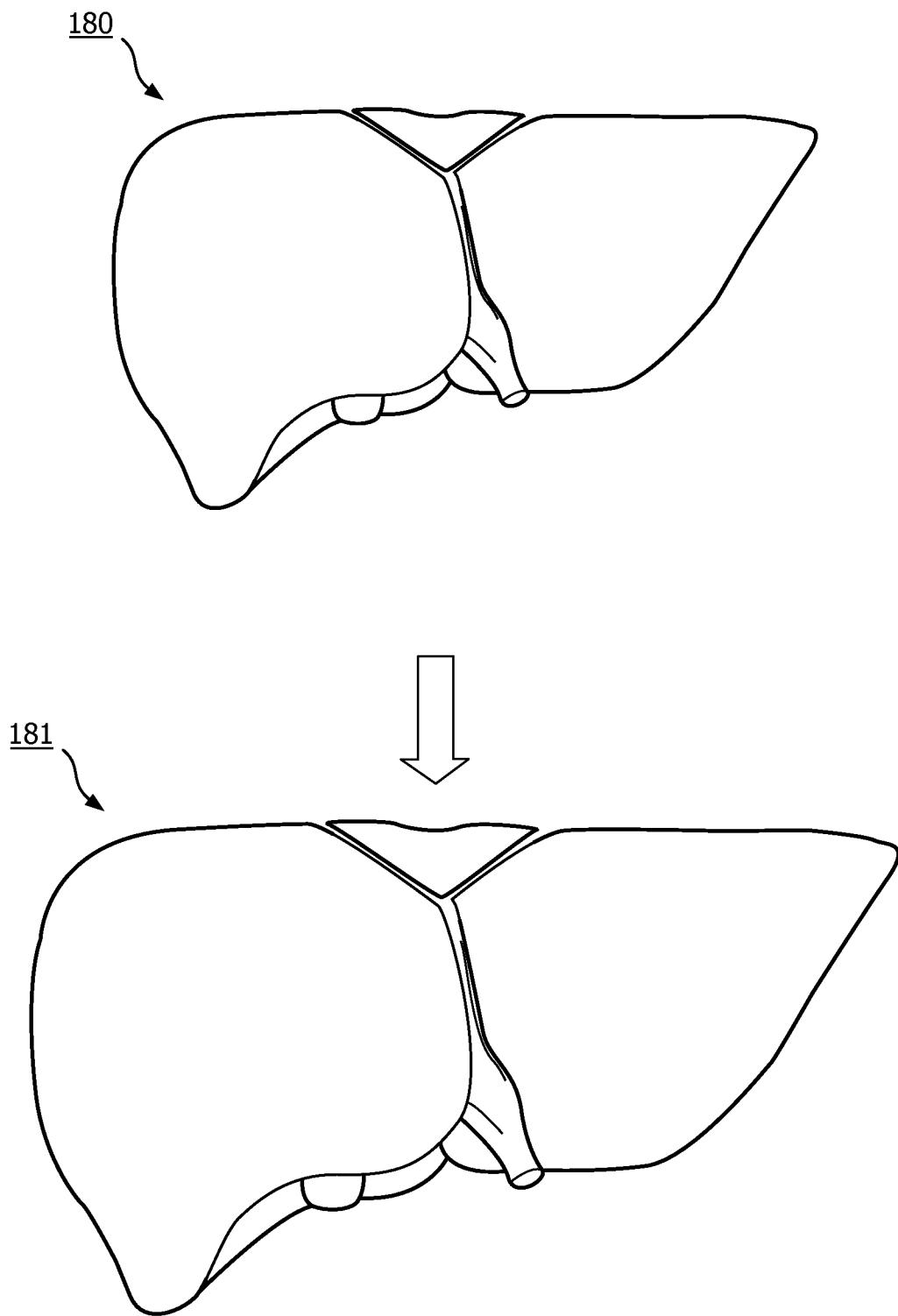


FIG. 7F

INTERNATIONAL SEARCH REPORT

International application No
PCT/EP2018/058379

A. CLASSIFICATION OF SUBJECT MATTER
 INV. A61B90/00 A61B34/30 A61B5/00 G01B5/008 G01B3/00
 ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
A61B G01B G06T

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2012/316827 A1 (WILKINSON MATTHEW TYLER [US] ET AL) 13 December 2012 (2012-12-13) paragraphs [0038] - [0042], [0049] - [0055] figures 6, 7, 9, 10 -----	1-5,9-14
X	US 2013/138404 A1 (CARBONERA CARLOS [US] ET AL) 30 May 2013 (2013-05-30) paragraphs [0035] - [0072] figures 1, 3, 5-8, 10 -----	1-6,9-14
A	EP 2 179 703 A1 (BRAINLAB AG [DE]) 28 April 2010 (2010-04-28) figure 2 -----	1-15
A	DE 102 58 579 A1 (CARL MAHR HOLDING GMBH [DE]) 8 July 2004 (2004-07-08) figure 6 -----	1-15
	-/-	

Further documents are listed in the continuation of Box C.

See patent family annex.

* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier application or patent but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search	Date of mailing of the international search report
12 June 2018	20/06/2018
Name and mailing address of the ISA/ European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Fax: (+31-70) 340-3016	Authorized officer Mathis, Martin

INTERNATIONAL SEARCH REPORT

International application No
PCT/EP2018/058379

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 2012/125811 A1 (SIEMENS CORP [US]; PALADINI GIANLUCA [US]) 20 September 2012 (2012-09-20) figures 7,8 -----	1-15
E	US 2018/149460 A1 (MCGUIRE JONATHAN G [US] ET AL) 31 May 2018 (2018-05-31) the whole document -----	1-15

INTERNATIONAL SEARCH REPORT

International application No.
PCT/EP2018/058379

Box No. II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. Claims Nos.: **16-20**
because they relate to subject matter not required to be searched by this Authority, namely:
see FURTHER INFORMATION sheet PCT/ISA/210
2. Claims Nos.:
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:
3. Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box No. III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2. As all searchable claims could be searched without effort justifying an additional fees, this Authority did not invite payment of additional fees.
3. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:
4. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

The additional search fees were accompanied by the applicant's protest and, where applicable, the payment of a protest fee.

The additional search fees were accompanied by the applicant's protest but the applicable protest fee was not paid within the time limit specified in the invitation.

No protest accompanied the payment of additional search fees.

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box II.1

Claims Nos.: 16-20

The force sensed surface scanning method as defined in claims 16-20 comprise the steps of controlling a surface scanning of an anatomical organ by applying a contact force to the anatomical organ for constructing an intraoperative volume model of the anatomical organ. Hence, they relate to methods for treatment of the human or animal body by surgery. The International Searching Authority is not required to search such claims in terms of Rule 39.1(iv) PCT.

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No PCT/EP2018/058379

Patent document cited in search report	Publication date	Patent family member(s)			Publication date
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		WO 2018102448 A1			07-06-2018
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