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(73) Patenthaver: **The Good Ear Company, Inc., 24811 Magic Mtn Pkwy, 1631, Valencia, CA 91355, USA**

(72) Opfinder: **Kwak, Sangyeop, 105-902, Seo-gang LG Apt., Shin-jeong dong Mapo-gu, Seoul, Sydkorea**

(74) Fuldmægtig i Danmark: **Michalski Hüttermann & Partner Patentanwälte mbH, Speditionstraße 21, 40221 Düsseldorf, Tyskland**

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DESCRIPTION

BACKGROUND OF THE INVENTION

[0001] The present invention relates to a recording media for hair cell stimulation using acoustic signals. More particularly, the present invention relates to a recording media for diagnosing accurately hearing ability of a user and improving the hearing ability on the basis of the diagnosed result.

[0002] Every organ for delivering sound to a brain is referred to as an auditory organ.

[0003] The auditory organ is divided into an outer ear, a middle ear and an inner ear. Sound inputted from an outside through the outer ear vibrates a tympanic membrane, and then the sound is delivered to a cochlea of the inner ear via the middle ear.

[0004] Auditory hair cells are arranged on a basilar membrane of the cochlea. Here, the number of the hair cells arranged on the basilar membrane is approximately 12,000.

[0005] The basilar membrane has length of approximately 2.5 to 3cm. The hair cell located on an initial part of the basilar membrane senses high frequency-sound, and the hair cell located on an end of the basilar membrane senses low frequency-sound. This is referred to as frequency specificity of the hair cell. Generally, resolution of the frequency specificity corresponding to ideal stimulation intensity equals to approximately 0.2mm (0.5 semitone) on the basilar membrane.

[0006] Recently, since use of a portable acoustic device has been increased and people are exposed to various noises, many people have sensorineural hearing loss.

[0007] The sensorineural hearing loss is a hearing ability degeneration phenomenon caused by the hair cell damage, and is generated by aging, noise exposure, drug side effect, genetic cause, etc.

[0008] Based on the severity, the sensorineural hearing loss is divided into mild hearing loss, moderate hearing loss, severe hearing loss and profound hearing loss. Generally, people who have more severe hearing loss than moderate level are hard to have a normal conversation.

[0009] Currently, it is estimated that about ten percent of total world population has the mild hearing loss in which people feel degeneration of their hearing ability. In addition, it is estimated that approximately 260,000,000 people or more have the moderate hearing loss, the severe hearing loss or the profound hearing loss in only developing countries.

[0010] However, a method for treatment of the hearing loss is not existed, but only a hearing

aid is provided as an alternative device related to the hearing loss.

[0011] The hearing aid simply amplifies external sound so that the sound is heard, and thus the hearing aid may not prevent degeneration of the hearing ability. Specially, a problem exists in that the hearing ability of the hearing aid user is more degenerated due to the amplified sound.

[0012] Accordingly, a method for fundamental treatment of the hearing loss has been required.

[0013] As for a diagnostic method of hearing loss, pure-tone audiometry, which uses the frequency specificity of hair cells, is widely used as international standard hearing test method.

[0014] The conventional pure-tone audiometry divides uniformly the basilar membrane into six parts through one octave interval resolution, and observes the frequency specificity of the hair cells located on each of the six parts with six frequency (for example 250, 500, 1000, 2000, 4000 and 8000Hz) signals.

[0015] In case that normal frequency specificity is observed because the hair cell is not damaged, the frequency specificity of the hair cell may be induced in response to the signal with small sound pressure intensity.

[0016] For example, in case that the frequency specificity of the hair cell corresponding to 1000Hz is normal, electrical reaction to -1.4dBSPL (sound pressure level) 1000Hz pure-tone stimulus may be induced in the hair cell.

[0017] In conventional technique, to diagnose hearing ability, a skilled examiner presents acoustic signals corresponding to the parts divided with only one octave resolution to a subject using a complex diagnostic device. The subject pushes a response button when he can hear the presented signal. Because of the low frequency resolution of the conventional audiometry, it is difficult to diagnose accurately the hearing ability. Additionally, the conventional technique is inconvenient to diagnose the hearing ability.

[0018] Patent US 3,531,595 is about multi-channel hearing aid. Multi-channel hearing aid can be regarded as a series of multi-channel amplifiers to compensate hearing deficiencies frequency-specifically.

[0019] On the other hand, US laid-open 2006-167335 is about 'audiogram based TRT (tinnitus retraining therapy)'. They adopt only white noise (broad-band noise) as a stimulus for masking tinnitus, and their white noise stimulus which has a frequency equalized characteristics based on user's audiogram, plays a role as only a tinnitus masker.

SUMMARY OF THE INVENTION

[0020] Accordingly, the present invention is provided to substantially obviate one or more problems due to limitations and disadvantages of the related art.

[0021] The present invention thus provides a recording media for hair cell stimulation using acoustic signals so as to improve hearing loss and is defined by the appended claims.

[0022] It is another feature of the present invention to provide a recording media for hair cell stimulation using acoustic signals to diagnose more accurately hearing ability of a user.

[0023] It is still another feature of the present invention to provide a recording media for hair cell stimulation using acoustic signals to diagnose accurately hearing ability of a user at a remote place and to provide a service for improvement of hearing loss.

[0024] A recording media readable by a computer and having a program of commands executed by the computer for the purpose of stimulating hair cell using acoustic stimulation, wherein the computer is connected to a user input section, a display section an apparatus for hair cell stimulation by acoustic signals, said apparatus comprising:- a hearing diagnosis section (100) configured to measure hearing threshold of a hair cell region on the basis of a user's response information on a specific acoustic signal;- a stimulation region detecting section (102) configured to determine a frequency band corresponding to damaged hair cell region as a target frequency band using the measured hearing threshold; and- a stimulation treatment section (104) configured to output an acoustic signal with preset intensity to the determined target frequency band, and characterized in that the program of commands is adapted to cause the computer to perform a method comprising the steps of:(a) determining with the hearing diagnosis section (100) of a hair cell stimulation apparatus, a frequency band corresponding to a damaged hair cell region by outputting a cochlear model interface that is output by the display section (232) of the computer includes hair cell region images (300) divided with 1/k octave resolution, wherein the k is a positive integer of above 2, and when a user selects at least one of the hair cell region images, outputting a diagnostic acoustic signal with a frequency band corresponding to the selected hair cell region image and determining a hearing threshold using a user's response information from the output diagnostic acoustic signal via the user input section; and(b) determining with the stimulation region detecting section (102) of the hair cell stimulation apparatus, a frequency band of a hair cell region in which hearing threshold of the corresponding frequency band selected from the hair cell region images (300) is higher than a preset reference value as the target frequency band corresponding to the damaged hair cell region; and(c) outputting with a stimulation treatment section of the hair cell stimulation apparatus, a stimulating acoustic signal to the target frequency band at a preset intensity to stimulate the damaged hair cell region, wherein the preset intensity is approximately by 3dB to 20dB higher than the hearing threshold of the damaged hair cell region, wherein the stimulating acoustic signal is at least one of amplitude modulated tone, frequency modulated tone, pulse tone, continuous tone, and amplitude modulated narrowband noise, or combination of the tones and the noise.

[0025] As described above, in a recording media for hair cell stimulation of the present

invention, a user may diagnose easily and accurately hearing ability through cochlear model interface.

[0026] In a recording media for hair cell stimulation of the present invention, a user may verify visually acoustic signal stimulation and the amount of improvement hearing ability.

[0027] A recording media for hair cell stimulation of the present invention may improve fundamentally hearing ability.

BRIEF DESCRIPTION OF THE DRAWINGS

[0028] Example embodiments of the present invention will become more apparent by describing in detail example embodiments of the present invention with reference to the accompanying drawings, in which:

FIG. 1 is a block diagram illustrating an apparatus for hair cell stimulation according to one example embodiment of the present invention;

FIG. 2 is a detail block diagram illustrating an apparatus for hair cell stimulation according to one example embodiment of the present invention;

FIG. 3 is a view illustrating cochlear model interface according to one example embodiment of the present invention;

FIG. 4 is a flow chart illustrating a diagnostic process of the hearing ability according to one example embodiment of the present invention;

FIG. 5 is a flow chart illustrating a process of hair cell stimulation according to one example embodiment of the present invention;

FIG. 6 is a view illustrating a hearing improvement service system according to one example embodiment of the present invention;

FIG. 7 is a view illustrating a graph indicating pure-tone audiometry result of one subject;

FIG. 8 is a view illustrating the target frequency band determined for the subject in FIG. 7;

FIG. 9 is a view illustrating schedule for acoustic signal stimulation;

FIG. 10 is a graph showing hearing threshold of the right ear before and after the acoustic signal stimulation is provided;

FIG. 11 is a view illustrating schedule for verifying whether or not the hearing ability improvement is continuously maintained after the acoustic signal stimulation to the right ear is stopped;

FIG. 12 is a view illustrating a graph corresponding to a table 3.

DESCRIPTION OF SPECIFIC EMBODIMENTS

[0029] Example embodiments of the present invention are disclosed herein. However, specific structural and functional details disclosed herein are merely representative for purposes of describing example embodiments of the present invention, however, example embodiments of the present invention may be embodied in many alternate forms and should not be construed as limited to example embodiments of the present invention set forth herein.

[0030] Accordingly, while the invention is susceptible to various modifications and alternative forms, specific embodiments thereof are shown by way of example in the drawings and will herein be described in detail. It should be understood, however, that there is no intent to limit the invention to the particular forms disclosed, but on the contrary, the invention is to cover all modifications, equivalents, and alternatives falling within the scope of the invention. Like numbers refer to like elements throughout the description of the figures.

[0031] It will be understood that, although the terms first, second, etc. may be used herein to describe various elements, these elements should not be limited by these terms. These terms are only used to distinguish one element from another. For example, a first element could be termed a second element, and, similarly, a second element could be termed a first element, without departing from the scope of the present invention. As used herein, the term "and/or" includes any and all combinations of one or more of the associated listed items.

[0032] It will be understood that when an element is referred to as being "connected" or "coupled" to another element, it can be directly connected or coupled to the other element or intervening elements may be present. In contrast, when an element is referred to as being "directly connected" or "directly coupled" to another element, there are no intervening elements present. Other words used to describe the relationship between elements should be interpreted in a like fashion (i.e., "between" versus "directly between", "adjacent" versus "directly adjacent", etc.).

[0033] The terminology used herein is for the purpose of describing particular embodiments only and is not intended to be limiting of the invention. As used herein, the singular forms "a", "an" and "the" are intended to include the plural forms as well, unless the context clearly indicates otherwise. It will be further understood that the terms "comprise", "comprising,", "include" and/or "including", when used herein, specify the presence of stated features, integers, steps, operations, elements, and/or components, but do not preclude the presence or addition of one or more other features, integers, steps, operations, elements, components, and/or groups thereof.

[0034] Unless otherwise defined, all terms (including technical and scientific terms) used

herein have the same meaning as commonly understood by one of ordinary skill in the art to which this invention belongs. It will be further understood that terms, such as those defined in commonly used dictionaries, should be interpreted as having a meaning that is consistent with their meaning in the context of the relevant art and will not be interpreted in an idealized or overly formal sense unless expressly so defined herein.

[0035] FIG. 1 is a block diagram illustrating an apparatus for hair cell stimulation according to one example embodiment of the present invention.

[0036] In FIG. 1, the apparatus for hair cell stimulation of the present embodiment includes a hearing diagnosis section 100, a stimulation region detecting section 102 and a stimulation treatment section 104.

[0037] The hearing diagnosis section 100 provides an acoustic signal corresponding to specific frequency band to a user, and measures the hearing ability of a user at the frequency band through the user's response on the provided acoustic signal. Here, the hearing ability may be measured through a pure-tone audiometry (PTA), an otoacoustic emission (OAE), an evoked response audiometry (ERA), etc.

[0038] In the embodiment of the present invention, unlike the conventional method with one octave frequency resolution, the hearing diagnosis section 100 provides the acoustic signal of the frequency band divided with resolution smaller than one octave resolution to the user, and detects location of damaged hair cells and the extent of the damage.

[0039] The hearing diagnosis section 100 provides the acoustic signal of the frequency band with 1/k (is positive integer of above 2) octave resolution, more preferably 1/3 to 1/24 octave resolution to the user, and diagnoses hearing ability of the user. Here, in one example embodiment of the present invention, the acoustic signal provided to the user corresponds to a medium frequency in a range of 250Hz to 12000 Hz. In case of dividing the medium frequency range with maximum 1/24 octave resolution, whole hair cell region of the user may be divided into 134 frequency bands (134 hair cell regions).

[0040] During the hearing diagnosis, the acoustic signal of specific frequency band selected from 134 frequency bands is provided to the user, and the user inputs his response information on the provided acoustic signal of which volume is adjusted.

[0041] The user's response information on the volume adjustment is stored as hearing threshold corresponding to the acoustic signal of the selected frequency band. Here, the hearing threshold of a frequency band means a hearing threshold of the hair cell region having frequency specificity on the selected frequency band.

[0042] The simulation region detecting section 102 detects a simulation region using the hearing threshold of each frequency band. Here, the detection of the simulation region indicates detection of the hair cell region to which acoustic signal stimulation is to be provided.

Particularly, the detection of the simulation region determines the frequency band corresponding to a damaged hair cell region.

[0043] The simulation treatment section 104 outputs the acoustic signal with preset intensity to the frequency band of the damaged hair cell region which is determined by the stimulation region detecting section 102. Here, the acoustic signal is provided with intensity higher by predetermined level than the hearing threshold of corresponding frequency band, which is pre-stored in the hearing diagnosis section 100.

[0044] In the present invention, the acoustic signal corresponds to at least one of amplitude modulated tone, frequency modulated tone, pulse tone and amplitude modulated narrowband noise, or combination of the tones and the noise.

[0045] Furthermore, in case that several hair cell regions are damaged, the acoustic signal may be provided to the damaged hair cell regions in an order of damage severity, be provided randomly to the damaged hair cell regions, or be provided simultaneously to the damaged hair cell regions.

[0046] In case that the acoustic signal is provided to the damaged hair cell regions of the user with various intensities, types or orders, the user's hearing ability may be improved.

[0047] Hereinafter, the apparatus for hair cell stimulation of the present embodiment will be described in detail with reference to accompanying drawing FIG. 2.

[0048] FIG. 2 is a detail block diagram illustrating an apparatus for hair cell stimulation according to one example embodiment of the present invention.

[0049] As shown in FIG. 2, the hearing diagnosis section 100 of the present embodiment includes an UI output section 200 and a response information storage section 202.

[0050] In one example embodiment of the present invention, the UI output section 200 displays cochlear model interface shown in FIG 3 on a display section 232 so that the subject not a skilled expert can diagnose his hearing ability by himself.

[0051] As shown in FIG. 3, the cochlear model interface of the present embodiment has an image 300 corresponding to the hair cell regions divided with high resolution. Here, since whole frequency range for hearing diagnosis corresponds to the medium frequency, i.e. 250Hz to 12000Hz, the cochlear model interface may have 134 hair cell region images 300 in case of dividing the medium frequency range with 1/24 octave resolution.

[0052] In case that the user selects one of the hair cell region images 300 in order to measure the hearing ability, an acoustic signal of a frequency band matched with the selected hair cell region image is outputted. Here, the frequency band matched with the hair cell region image means the frequency band to which corresponding hair cell region has frequency specificity. In

addition, the hair cell region image 300 may be selected by using a key button, a mouse, a touch screen method, etc.

[0053] In case that the acoustic signal is outputted, the user may adjust intensity of the acoustic signal using volume control 302, and inputs response information about an intensity point at which the acoustic signal is not heard.

[0054] The response information storage section 202 receives the response information corresponding to each of the acoustic signals from a user input section 220, and stores the received response information. Here, the user input section 220 may be a keypad, a mouse or a touch screen. In one example embodiment of the present invention, the response information may be stored as the hearing threshold of the frequency band related to corresponding acoustic signal as mentioned above.

[0055] The hearing diagnosis on several hair cell regions may be performed by the above method.

[0056] In FIG. 2, the stimulation region detecting section 102 includes a hearing threshold comparison section 204 and a target frequency band determining section 206.

[0057] The hearing threshold comparison section 204 compares the user's hearing threshold stored in the response information storage section 202 with a reference hearing threshold.

[0058] The hearing threshold comparison section 204 discriminates whether or not the hearing threshold of the measured frequency band is higher than the reference hearing threshold.

[0059] Based on the comparison result, the target frequency band determining section 206 determines a frequency band which requires treatment as a target frequency band. Here, the determination of the target frequency band indicates detection of damaged hair cell region, and the target frequency band may be determined in a unit of 1/k octave resolution like in the hearing diagnosis section 100. However, the determination of the target frequency band is not limited as the above method. For example, a frequency band range corresponding to the adjacent hair cell regions, in which the hair cell regions have high hearing threshold region, may be determined as the target frequency band.

[0060] Information about one or more target frequency band determined as above and information about order of damage severity are stored in the memory 208 in accordance with user identification information.

[0061] The stimulation treatment section 104 of the present embodiment includes an acoustic signal intensity determining section 210, an acoustic signal type determining section 212, a stimulation order determining section 214, an acoustic signal output section 216 and a timing section 218, and provides the acoustic signal to the user using the information stored in the memory 208.

[0062] The acoustic signal intensity determining section 210 determines intensity of the acoustic signal to be provided to the user.

[0063] The acoustic signal intensity determining section 210 determines intensity higher by 3 decibel to 20 decibel than the hearing threshold of each target frequency band as the acoustic signal intensity of the corresponding target frequency band.

[0064] In case that the target frequency band is determined as the frequency band range corresponding to the hair cell regions located continuously, the acoustic signal intensity determining section 210 may determines intensity higher by 3 decibel to 20 decibel than average value of the hearing thresholds of the hair cell regions as the acoustic signal intensity.

[0065] More preferably, the acoustic signal intensity may be determined in a range of 3 decibel to 10 decibel.

[0066] Considering user's preference, hearing loss severity, or target frequency band, the acoustic signal type determining section 212 determines type of the acoustic signal to be provided to the user.

[0067] In one example embodiment of the present invention, source of the acoustic signal may include amplitude modulated tone, frequency modulated tone, continuous tone, pulse tone, amplitude modulated narrowband noise, etc. Here, the acoustic signal type determining section 212 determines at least one of the tones and the noise or combination of the tones and the noise as the acoustic signal to be provided to the user.

[0068] Considering user's preference, hearing loss severity, or adjacency of the target frequency bands, the simulation order determining section 214 determines output order of the acoustic signals corresponding to several target frequency bands.

[0069] Preferably, the stimulation order determining section 214 may determine the output order so that the acoustic signal is outputted in sequence from the frequency band corresponding to the most damaged hair cell region. However, the above output order is not limited as the order mentioned above. For example, the acoustic signal may be randomly outputted, or be simultaneously outputted to the several target frequency bands.

[0070] The acoustic signal output section 216 outputs the acoustic signal with the determined intensity, type and order. Here, in case that the several target frequency bands are existed and the acoustic signals of the target frequency bands are individually outputted, output time of the each acoustic signal may be set. The timing section 218 detects whether or not the output time of the each acoustic signal is finished, and controls the acoustic signal output section 216 in accordance with the detection result so that the acoustic signal output section 216 outputs an acoustic signal of next target frequency band or finishes output of the acoustic signal.

[0071] In one example embodiment of the present invention, the UI output section 200 displays information on the cochlear model interface when the acoustic signal for hearing treatment of the user is outputted, wherein the user visually recognizes presence or absence, intensity, type, etc of the acoustic signal through the information.

[0072] For example, the UI output section 200 may change color or size of the hair cell region image 300 corresponding to the frequency band (target frequency band) of the acoustic signal outputted now in accordance with control of a controller 230.

[0073] In case that the acoustic signal is the amplitude modulated tone, the UI output section 200 may change color or size of corresponding hair cell region image 300 synchronizing with amplitude change of the amplitude modulated tone.

[0074] In case that the acoustic signal is the frequency modulated tone, the UI output section 200 may change color or size of the hair cell region image 300 corresponding to the changed frequency synchronizing with frequency change of the frequency modulated tone.

[0075] In case that the acoustic signal is the continuous tone or the pulse tone, the UI output section 200 may change color or size of corresponding hair cell region image 300 so that the user recognizes the currently provided acoustic signal as the continuous tone or the pulse tone.

[0076] In one example embodiment of the present invention, the user may verify intuitively through the cochlear model interface whether or not the hearing ability of each hair cell region is improved.

[0077] The UI output section 200 exhibits the hair cell region image 300 of the target frequency band differently from other hair cell image. Additionally, the UI output section 200 may indicate the image 300 of the damaged hair cell region with color or size varied in accordance with damage severity.

[0078] After the above stimulation through the acoustic signal (hereinafter, referred to as "acoustic signal stimulation"), the UI output section 200 changes color or size of corresponding hair cell region image 300 in accordance with the extent of improvement of each hair cell region so that the user recognizes the extent of hearing improvement.

[0079] The extent of hearing improvement may be discriminated by measuring again hearing threshold of the target frequency band.

[0080] Hereinafter, a method for hearing diagnosis and a method for hearing improvement of the present invention will be described in detail with reference to accompanying drawings FIG. 4 and FIG. 5.

[0081] FIG. 4 is a flow chart illustrating a diagnostic process of hearing ability according to one

example embodiment of the present invention. In this example, the display section 232 of the apparatus for hair cell stimulation is embodied with a touch screen.

[0082] Referring to FIG. 4, the apparatus for hair cell stimulation displays the cochlear model interface shown in FIG. 3 on the touch screen 232 in case that the user requests diagnosis of his hearing ability in step. Here, the cochlear model interface has several hair cell region images in which frequency bands generated by dividing medium frequency with maximum 1/24 octave resolution are visualized.

[0083] In step S402, it is discriminated whether or not the user selects the hair cell region image 300 displayed on the cochlear model interface.

[0084] In step S404, in case that the user selects the hair cell region image 300, an acoustic signal of the frequency band corresponding to the hair cell region related to the selected image 300 is outputted.

[0085] In step S406, the apparatus for hair cell stimulation discriminates whether or not the user's response information on the acoustic signal is received.

[0086] The user may adjust volume in accordance with whether or not the user hears the acoustic signal, and input the response information on the intensity level at which the acoustic signal is not heard.

[0087] In step S408, the user's response information is stored as the hearing threshold of the frequency band corresponding to each of the acoustic signals.

[0088] In step S410, the apparatus for hair cell stimulation compares the user's hearing threshold with the reference hearing threshold after the response information input is finished.

[0089] In step S412, the target frequency band is determined by the result of comparison between hearing thresholds, wherein the acoustic signal stimulation is required for the target frequency band.

[0090] In step S414, information concerning the target frequency band is stored in the memory 208. Here, the information concerning the target frequency band may include user identification information, hearing threshold information of the frequency band on which hearing diagnosis is performed, target frequency band information, order information on damage severity, etc.

[0091] In case that the acoustic signals are divided with 1/24 octave resolution, the target frequency band may be determined to the corresponding individual frequency band of each acoustic signal. However, the determination of the target frequency band is not limited as the above method. That is, specific frequency band range in which average of hearing thresholds of the frequency bands is higher than a reference value may be determined as the target

frequency band. For example, in case of measuring the hearing ability using each of the acoustic signals corresponding to the frequency bands of 5920Hz to 6093Hz (first interval), 6093Hz to 6272Hz (second interval) or 6272Hz to 6456Hz (third interval) generated by dividing the medium frequency with 1/24 octave resolution, the target frequency band may be determined in a unit of intervals or in new interval having the above three intervals, i.e. 5920Hz to 6456Hz.

[0092] FIG. 5 is a flow chart illustrating a process of hair cell stimulation according to one example embodiment of the present invention.

[0093] After the target frequency band is determined as mentioned above, the apparatus for hair cell stimulation determines intensity, type, order, etc of the target frequency band, and outputs the acoustic signal for improving the hearing ability of the user in accordance with the determination result.

[0094] Referring to FIG. 5, in case that the user requests presentation of the acoustic signal in step S500, the apparatus for hair cell stimulation reads information concerning the target frequency band from the memory 208 and then determines intensity of the acoustic signal of the target frequency band in step S502.

[0095] In steps S504 and S506, type and output order of the acoustic signal are determined.

[0096] As described above, the output order of the acoustic signal may be determined in accordance with damage severity, or be determined so that the acoustic signal is randomly or simultaneously outputted.

[0097] In step S508, the acoustic signal is outputted in accordance with the determined intensity, type and order.

[0098] In step S510, in case that the acoustic signal is outputted in accordance with damage severity or is randomly outputted, the apparatus for hair cell stimulation discriminates whether or not output time of one acoustic signal is finished.

[0099] In step S512, in case that the output time is finished, another acoustic signal corresponding to next target frequency band is outputted.

[0100] On the other hand, in case that the acoustic signal is outputted, the apparatus for hair cell stimulation synchronizes the cochlear model interface with output, amplitude change, frequency change or pulse period of the acoustic signal, and changes color or size of the hair cell region image 300 of the cochlear model interface in accordance with the synchronization.

[0101] The method for hair cell stimulation of the present embodiment is provided through a computer or a portable terminal established by the user or in a hospital, etc. In addition, the method may be provided through a network at a remote place.

[0102] FIG. 6 is a view illustrating a hearing improvement service system according to one example embodiment of the present invention.

[0103] In FIG. 6, the hearing improvement service system of the present embodiment includes a hearing improvement sever 600 connected electrically to at least one user client 602 through a network. Here, the network includes a wire network having an Internet and a private line and a wireless network having a wireless Internet, a mobile communication network and a satellite network.

[0104] The hearing improvement sever 600 provides an application for outputting the cochlear model interface shown in FIG. 3 to the user client 602 in accordance with request of the user. Here, the hearing improvement sever 600 may provide the application through various methods such as a download, webpage-inserted form, etc.

[0105] In case that the user selects a certain hair cell region image 300 through the cochlear model interface, the above application outputs an acoustic signal of a frequency band corresponding to the hair cell region selected by the user.

[0106] Subsequently, in case that the user inputs the response information about an intensity level at which the acoustic signal is not heard in accordance with volume control of the acoustic signal, the user client 602 transmits the response information to the hearing improvement sever 600.

[0107] The hearing improvement sever 600 includes the stimulation region detecting section as shown in FIG. 1 and FIG. 2, and determines the target frequency band requiring treatment on the basis of the transmitted response information of the user.

[0108] Additionally, the hearing improvement sever 600 stores information concerning the target frequency band and determines intensity, type, order, etc of the target frequency band. In case that the user requests, the hearing improvement sever 600 provides the acoustic signal corresponding to the target frequency band to the user client 602 through the network in accordance with the determined result.

[0109] The user client 602 may be embodied with a terminal which operates the application and is equipped with a speaker, and include a desktop, a laptop, a mobile communication terminal, etc.

[0110] The user client 602 stimulates the hair cell of the user by outputting the acoustic signal provided from the hearing improvement sever 600.

[0111] The extent of hearing improvement by the apparatus for hair cell stimulation of the present embodiment is verified through an experiment.

[0112] FIG. 7 is a view illustrating a graph indicating pure-tone audiometry result of one subject. Particularly, FIG. 7 shows result generated by examining hearing ability in the range of 2000Hz to 8000Hz with 1/24 octave resolution using the hearing diagnosis section 100.

[0113] As shown in FIG. 7, right ear of the subject has mild to moderate hearing loss in a frequency region of 3000Hz to 7000Hz.

[0114] FIG. 8 is a view illustrating the target frequency band determined for the subject in FIG 7. Particularly, a frequency band range of 5920Hz to 6840Hz showing approximately 50dBHL of hearing threshold is determined as the target frequency band for the subject in FIG. 7.

[0115] The acoustic signal such as frequency modulated tone or amplitude modulated narrowband noise related to the target frequency band determined in FIG. 8 is provided to the right ear for thirty minutes in the morning and evening over fifteen days. Here, the intensity of the acoustic signal is adjusted to 5 dBSL (sensational level) to 10 dBSL.

[0116] FIG. 9 is a view illustrating schedule for acoustic signal stimulation. Particularly, hearing ability is measured before the acoustic signal stimulation is provided (first test), after providing the acoustic signal stimulation for ten days (second test), and after providing the acoustic signal stimulation for fifteen days (third test), and then hearing thresholds corresponding to the measurement are compared.

[0117] In each test, in order to avoid misinterpretation due to the experimental error, the hearing ability is measured ten times with 1/24 octave resolution and then average of the measured values is used as the hearing ability.

[0118] Table 1 is a a table in which hearing threshold measured before providing the acoustic signal stimulation to a right ear is compared with that measured after the acoustic signal stimulation is provided to the right ear for ten days. Table 2 is a table in which the hearing threshold measured after acoustic signal stimulation is provided to the right ear for ten days is compared with that measured after the acoustic signal stimulation is provided to the right ear for fifteen days.

Table 1: Hearing threshold result after 10 days

Right	Before												10 days After											
	I	II	III	IV	V	VI	VII	VIII	IX	X	A1	A2	I	II	III	IV	V	VI	VII	VIII	IX	X	A1	A2
4067	32.5	37.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	33.0		32.5	32.5	32.5	32.5	32.5	32.5	32.5	27.5	32.5	32.5	32.0	
4186	32.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5		32.5	32.5	32.5	32.5	32.5	27.5	27.5	27.5	32.5	32.5	31.0	
4309	32.5	32.5	32.5	32.5	32.5	27.5	32.5	32.5	27.5	32.5	31.5		32.5	32.5	32.5	27.5	27.5	27.5	27.5	27.5	32.5	27.5	29.5	
4435	32.5	37.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	32.5	33.0		32.5	32.5	32.5	32.5	32.5	27.5	32.5	27.5	37.5	32.5	32.0	
4565	32.5	37.5	37.5	37.5	37.5	32.5	37.5	37.5	32.5	37.5	36.0		37.5	37.5	37.5	37.5	37.5	32.5	32.5	32.5	37.5	32.5	35.5	
4699	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5		37.5	37.5	37.5	37.5	37.5	37.5	37.5	32.5	42.5	37.5	37.5	
4836	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	36.2	37.5	37.5	37.5	37.5	37.5	37.5	37.5	32.5	37.5	37.5	37.0	34.3
4978	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5		37.5	32.5	37.5	37.5	37.5	37.5	37.5	32.5	37.5	37.5	36.5	
5124	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5		37.5	32.5	32.5	32.5	37.5	37.5	32.5	37.5	37.5	37.5	35.5	
5274	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5		32.5	32.5	32.5	32.5	32.5	37.5	32.5	37.5	32.5	32.5	33.5	
5429	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5		32.5	32.5	32.5	32.5	37.5	37.5	32.5	37.5	32.5	32.5	34.0	
5588	42.5	37.5	42.5	37.5	42.5	37.5	37.5	37.5	37.5	42.5	39.5		37.5	37.5	37.5	32.5	37.5	37.5	37.5	37.5	32.5	37.5	36.5	

5752	42.5	37.5	42.5	37.5	42.5	37.5	37.5	42.5	37.5	42.5	40.0			27.5	37.5	37.5	32.5	37.5	37.5	37.5	37.5	32.5	37.5	35.5		
5920	42.5	37.5	42.5	42.5	42.5	37.5	37.5	42.5	42.5	42.5	41.0			37.5	37.5	37.5	32.5	37.5	42.5	37.5	42.5	32.5	37.5	37.5		
6093	42.5	42.5	42.5	42.5	42.5	42.5	42.5	47.5	42.5	47.5	43.5			37.5	37.5	37.5	37.5	37.5	42.5	37.5	37.5	32.5	37.5	37.5		
6272	47.5	42.5	47.5	42.5	47.5	47.5	42.5	47.5	42.5	47.5	45.5	45.4		37.5	42.5	37.5	37.5	37.5	42.5	42.5	42.5	32.5	37.5	38.0	38.2	
6456	52.5	42.5	47.5	47.5	47.5	47.5	42.5	47.5	47.5	47.5	47.0			37.5	42.5	42.5	37.5	37.5	42.5	42.5	47.5	32.5	42.5	40.5		
6645	52.5	42.5	52.5	42.5	52.5	47.5	42.5	42.5	57.5	47.5	50.0			37.5	42.5	42.5	37.5	37.5	42.5	37.5	42.5	32.5	37.5	38.0		
6840	47.5	42.5	47.5	42.5	47.5	47.5	42.5	42.5	52.5	42.5	45.5			37.5	37.5	37.5	37.5	37.5	37.5	37.5	42.5	32.5	37.5	36.5		
7040	42.5	37.5	42.5	37.5	42.5	37.5	37.5	37.5	42.5	37.5	39.5			32.5	32.5	32.5	32.5	37.5	37.5	37.5	37.5	32.5	32.5	34.5		
7246	37.5	32.5	37.5	32.5	37.5	37.5	32.5	32.5	37.5	32.5	35.0			32.5	32.5	32.5	27.5	32.5	32.5	32.5	32.5	27.5	32.5	31.5		
7459	27.5	27.5	32.5	27.5	32.5	27.5	27.5	27.5	27.5	27.5	28.5	30.0		27.5	27.5	22.5	22.5	27.5	27.5	27.5	27.5	27.5	27.5	26.5	27.3	
7677	27.5	22.5	27.5	22.5	27.5	22.5	22.5	22.5	27.5	22.5	24.5			22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5		
7902	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5			22.5	22.5	17.5	22.5	22.5	17.5	22.5	22.5	22.5	22.5	21.5		

Table 2: Hearing threshold result after 15 days

Right	10 days After												15 days After											
	I	II	III	IV	V	VI	VII	VIII	IX	X	A1	A2	I	II	III	IV	V	VI	VII	VIII	IX	X	A1	A2
4067	32.5	32.5	32.5	32.5	32.5	32.5	32.5	27.5	32.5	32.5	32.0		37.5	37.5	27.5	37.5	32.5	37.5	32.5	37.5	32.5	22.5	33.5	
4186	32.5	32.5	32.5	32.5	32.5	27.5	27.5	27.5	32.5	32.5	31.0		32.5	37.5	37.5	37.5	32.5	32.5	27.5	37.5	32.5	32.5	34.0	
4309	32.5	32.5	32.5	27.5	27.5	27.5	27.5	27.5	32.5	27.5	29.5		27.5	37.5	27.5	37.5	37.5	32.5	32.5	37.5	32.5	32.5	33.5	
4435	32.5	32.5	32.5	32.5	32.5	27.5	32.5	27.5	37.5	32.5	32.0		32.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	32.5	36.5	
4565	37.5	37.5	37.5	37.5	37.5	32.5	32.5	32.5	37.5	32.5	35.5		27.5	37.5	37.5	37.5	42.5	37.5	32.5	42.5	37.5	32.5	36.5	
4699	37.5	37.5	37.5	37.5	37.5	37.5	37.5	32.5	42.5	37.5	37.5		37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	
4836	37.5	37.5	37.5	37.5	37.5	37.5	37.5	32.5	37.5	37.5	37.0	34.3	37.5	37.5	22.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	36.0	34.5
4978	37.5	32.5	37.5	37.5	37.5	37.5	37.5	32.5	37.5	37.5	36.5		37.5	37.5	27.5	37.5	37.5	37.5	37.5	37.5	37.5	37.5	36.5	
5124	37.5	32.5	32.5	32.5	37.5	37.5	32.5	37.5	37.5	37.5	35.5		32.5	32.5	27.5	32.5	32.5	32.5	32.5	37.5	37.5	32.5	33.0	
5274	32.5	32.5	32.5	32.5	32.5	37.5	32.5	37.5	32.5	32.5	33.5		32.5	32.5	32.5	32.5	32.5	37.5	32.5	32.5	37.5	32.5	33.5	
5428	32.5	32.5	32.5	32.5	37.5	37.5	32.5	37.5	32.5	32.5	34.0		32.5	32.5	32.5	32.5	32.5	37.5	32.5	32.5	37.5	32.5	33.5	
5588	37.5	37.5	37.5	32.5	37.5	37.5	37.5	37.5	32.5	37.5	36.5		27.5	32.5	32.5	32.5	32.5	37.5	32.5	32.5	37.5	37.5	33.5	
5752	27.5	37.5	37.5	32.5	37.5	37.5	37.5	37.5	32.5	37.5	35.5		27.5	32.5	32.5	32.5	32.5	37.5	27.5	27.5	37.5	27.5	31.5	
5920	37.5	37.5	37.5	32.5	37.5	42.5	37.5	42.5	32.5	37.5	37.5		37.5	32.5	32.5	32.5	32.5	37.5	37.5	32.5	37.5	27.5	34.0	
6093	37.5	37.5	37.5	37.5	37.5	42.5	37.5	37.5	32.5	37.5	37.5		37.5	32.5	32.5	37.5	32.5	37.5	37.5	27.5	32.5	37.5	34.5	
6272	37.5	42.5	37.5	37.5	37.5	42.5	42.5	42.5	32.5	37.5	39.0	38.2	37.5	27.5	37.5	32.5	37.5	37.5	27.5	32.5	32.5	37.5	34.0	34.2
6456	37.5	42.5	42.5	37.5	37.5	42.5	42.5	47.5	32.5	42.5	40.5		37.5	32.5	37.5	37.5	37.5	37.5	37.5	32.5	32.5	32.5	35.5	
6645	27.5	42.5	42.5	37.5	37.5	42.5	37.5	42.5	32.5	37.5	38.0		27.5	32.5	32.5	32.5	32.5	37.5	37.5	32.5	37.5	32.5	33.5	
6840	27.5	37.5	37.5	37.5	37.5	37.5	37.5	42.5	32.5	37.5	36.5		32.5	32.5	32.5	37.5	37.5	37.5	27.5	32.5	37.5	32.5	34.0	
7040	32.5	32.5	32.5	32.5	37.5	37.5	37.5	37.5	32.5	32.5	34.5		32.5	32.5	27.5	32.5	32.5	32.5	32.5	27.5	37.5	27.5	31.5	
7246	32.5	32.5	32.5	27.5	32.5	32.5	32.5	32.5	27.5	32.5	31.5		32.5	32.5	27.5	27.5	32.5	32.5	32.5	32.5	32.5	27.5	31.0	
7459	27.5	27.5	22.5	22.5	27.5	27.5	27.5	27.5	27.5	27.5	26.5	27.3	22.5	27.5	27.5	27.5	27.5	27.5	27.5	22.5	27.5	27.5	26.5	26.3
7677	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5		22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	22.5	
7902	22.5	22.5	17.5	22.5	22.5	17.5	22.5	22.5	22.5	22.5	21.5		17.5	17.5	17.5	17.5	22.5	22.5	22.5	22.5	17.5	22.5	20.0	

[0119] Referring to Table 1 and 2, the hearing threshold of the target frequency band becomes lower after the acoustic signal stimulation is provided, i.e. the hearing ability is improved.

[0120] FIG. 10 is a view illustrating a graph showing the hearing threshold of the right ear before and after the acoustic signal stimulation is provided.

[0121] In FIG. 10, before the acoustic signal stimulation is provided, hearing threshold (right ear) of a frequency band of 5920Hz to 6840Hz equals to 45.4 dBHL. However, after the acoustic signal stimulation is provided for ten days, the hearing threshold of the frequency band is lowered to 38.2 dBHL. In addition, the hearing threshold is more lowered to 34.2 dBHL after the acoustic signal stimulation is provided for fifteen days.

[0122] The extent of the hearing threshold reduction is statistically significant.

[0123] FIG. 11 is a view illustrating schedule for verifying whether or not the hearing ability improvement is continuously maintained after the acoustic signal stimulation to the right ear is stopped.

[0124] The hearing ability is measured from five days to eighteen days after the acoustic signal stimulation is stopped.

[0125] Table 3 is a table showing hearing threshold of the right ear after the acoustic signal stimulation is stopped. FIG. 12 is a view illustrating a graph corresponding to the Table 3.

[0126] Referring to Table 3 and FIG. 12, the hearing ability improvement effect is maintained after the acoustic signal stimulation is stopped. Additionally, it is verified that the hearing ability is still improved by approximately 7.9 dB eighteen days after the acoustic signal stimulation is stopped.

Table 3: measurement result of the hearing ability after the stimulation is stopped

right	5 d			A2	6 d			A2	7 d			A2	8 d			A2	10 d			A2	12 d			A2	18 d			A2
4067	32.5	32.5	32.5		32.5	37.5	35.0		37.5	32.5	35.0		37.5	32.5	35.0		32.5	27.5	30.0		32.5	37.5	35.0		32.5	32.5	32.5	
4186	32.5	32.5	32.5		27.5	32.5	30.0		32.5	32.5	32.5		27.5	32.5	30.0		32.5	32.5	32.5		32.5	32.5	32.5		32.5	32.5	32.5	
4309	32.5	37.5	35.0		32.5	27.5	30.0		32.5	27.5	30.0		32.5	32.5	32.5		32.5	27.5	30.0		37.5	37.5	37.5		27.5	32.5	30.0	
4435	32.5	37.5	35.0		32.5	17.5	25.0		32.5	32.5	32.5		32.5	32.5	32.5		32.5	32.5	32.5		37.5	37.5	37.5		32.5	32.5	32.5	
4565	37.5	37.5	37.5		27.5	32.5	30.0		37.5	37.5	37.5		27.5	32.5	30.0		32.5	32.5	32.5		37.5	37.5	37.5		37.5	32.5	35.0	
4698	37.5	37.5	37.5		32.5	37.5	35.0		32.5	32.5	32.5		32.5	32.5	32.5		22.5	32.5	27.5		22.5	27.5	25.0		37.5	37.5	37.5	
4836	22.5	37.5	30.0	35.2	37.5	37.5	37.5	31.7	27.5	27.5	27.5	31.7	32.5	32.5	32.5	31.5	32.5	32.5	32.5	31.2	22.5	37.5	30.0	33.7	37.5	32.5	35.0	35.0
4978	27.5	37.5	32.5		32.5	32.5	32.5		22.5	32.5	27.5		32.5	32.5	32.5		32.5	32.5	32.5		37.5	37.5	37.5		32.5	37.5	35.0	
5124	37.5	37.5	37.5		27.5	32.5	30.0		37.5	27.5	32.5		22.5	27.5	25.0		27.5	32.5	30.0		37.5	27.5	32.5		37.5	37.5	37.5	
5274	37.5	37.5	37.5		32.5	32.5	32.5		37.5	32.5	35.0		32.5	32.5	32.5		32.5	27.5	30.0		37.5	27.5	32.5		37.5	37.5	37.5	
5428	37.5	37.5	37.5		32.5	32.5	32.5		22.5	27.5	25.0		32.5	32.5	32.5		32.5	32.5	32.5		32.5	32.5	32.5		37.5	32.5	35.0	
5568	37.5	37.5	37.5		32.5	32.5	32.5		37.5	32.5	35.0		32.5	27.5	30.0		32.5	27.5	30.0		37.5	32.5	35.0		37.5	37.5	37.5	
5752	32.5	37.5	35.0		27.5	32.5	30.0		37.5	22.5	30.0		32.5	32.5	32.5		32.5	32.5	32.5		32.5	32.5	32.5		37.5	37.5	37.5	
5920	42.5	37.5	40.0		22.5	27.5	25.0		37.5	32.5	35.0		32.5	32.5	32.5		32.5	32.5	32.5		37.5	32.5	35.0		32.5	37.5	35.0	
6093	27.5	37.5	32.5		32.5	32.5	32.5		37.5	27.5	32.5		27.5	32.5	30.0		27.5	32.5	30.0		37.5	32.5	35.0		37.5	37.5	37.5	
6272	42.5	37.5	40.0	39.2	32.5	32.5	32.5	30.0	37.5	37.5	37.5	35.0	32.5	32.5	32.5	30.9	37.5	37.5	37.5	35.4	37.5	32.5	35.0	36.3	37.5	42.5	40.0	37.5
6456	47.5	37.5	42.5		27.5	32.5	30.0		27.5	42.5	35.0		27.5	37.5	32.5		37.5	37.5	37.5		37.5	37.5	37.5		37.5	37.5	37.5	
6645	42.5	37.5	40.0		37.5	27.5	32.5		42.5	37.5	40.0		32.5	27.5	30.0		37.5	37.5	37.5		37.5	37.5	37.5		37.5	37.5	37.5	
6840	42.5	37.5	40.0		27.5	27.5	27.5		22.5	37.5	30.0		32.5	22.5	27.5		37.5	37.5	37.5		37.5	37.5	37.5		37.5	37.5	37.5	
7040	37.5	37.5	37.5		32.5	32.5	32.5		37.5	37.5	37.5		32.5	32.5	32.5		32.5	32.5	32.5		32.5	32.5	32.5		37.5	37.5	37.5	
7246	32.5	32.5	32.5		32.5	27.5	30.0		27.5	32.5	30.0		27.5	27.5	27.5		32.5	27.5	30.0		32.5	27.5	30.0		32.5	32.5	32.5	
7459	27.5	22.5	25.0	28.5	12.5	27.5	20.0	24.5	27.5	27.5	27.5	27.5	22.5	22.5	22.5	24.5	27.5	22.5	25.0	26.0	27.5	27.5	27.5	27.0	27.5	27.5	27.5	28.5
7677	27.5	22.5	25.0		22.5	22.5	22.5		22.5	22.5	22.5		22.5	22.5	22.5		22.5	22.5	22.5		22.5	22.5	22.5		22.5	22.5	22.5	
7902	22.5	22.5	22.5		17.5	17.5	17.5		22.5	17.5	20.0		17.5	17.5	17.5		17.5	22.5	20.0		22.5	22.5	22.5		22.5	22.5	22.5	

[0127] Any reference in this specification to "one embodiment," "an embodiment," "example embodiment," etc., means that a particular feature, structure, or characteristic described in connection with the embodiment is included in at least one embodiment of the invention. The appearances of such phrases in various places in the specification are not necessarily all referring to the same embodiment. Further, when a particular feature, structure, or characteristic is described in connection with any embodiment, it is submitted that it is within the purview of one skilled in the art to affect such feature, structure, or characteristic in

connection with other ones of the embodiments.

[0128] Although embodiments have been described with reference to a number of illustrative embodiments thereof, it should be understood that numerous other modifications and embodiments can be devised by those skilled in the art that will fall within the scope of the principles of this disclosure. More particularly, various variations and modifications are possible in the component parts and/or arrangements of the subject combination arrangement within the scope of the disclosure, the drawings and the appended claims. In addition to variations and modifications in the component parts and/or arrangements, alternative uses will also be apparent to those skilled in the art.

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US3531595A [0018]
- US2006167335A [0019]

Apparat til stimulering af hårceller ved hjælp af akustiske signaler

Krav

1. Et registreringsmedie, der kan læses af en computer og som har et kommandoprogram, der udføres af computeren med det formål at stimulere hårceller ved hjælp af akustisk stimulering, hvor computeren er sluttet til en brugerindlæsesektion, en visningssektion for et apparat til stimulering af hårceller ved hjælp af akustiske signaler. Det nævnte apparat består af:

- En hørediagnosesektion (100), der er konfigureret til at måle høretærskel for et hårcelleområde på basis af en brugers responsinformation om et specifikt akustisk signal;
- en sektion til stimulering af et område (102), der er konfigureret til at bestemme et frekvensbånd, der svarer til et beskadiget hårcelleområde som et målfrekvensbånd ved hjælp af den målte høretærskel; og
- en stimuleringsbehandlingssektion (104), der er konfigureret til at udlæse et akustisk signal med forudindstillet intensitet til det bestemte målfrekvensbånd og

karakteriseret ved at kommandoprogrammet er tilpasset til at få computeren til at udføre en metode, der består af trinene for:

(a) bestemmelse med hørediagnosesektionen (100) i et hårcellestimuleringsapparat, et frekvensbånd, der svarer til et beskadiget hårcelleområde ved at udlæse en cochlear-modelgrænseflade, der udlæses af computerens visningssektion (232), omfatter hårcelleområdebilleder (300) delt med 1/k oktavopløsning, hvor k'et er et positivt heltal over 2, og når en bruger vælger mindst et af hårcellområdebillederne, der udlæser et diagnostisk akustisk signal med et frekvensbånd, der svarer til det valgte hårcelleområdebillede og bestemmer en høretærskel ved hjælp af en brugers responsinformation fra det udlæste diagnostiske akustiske signal via brugerindlæsesektionen; og

(b) bestemmelse med stimuleringsområdets registreringssektion (102) i hårcellestimuleringsapparatet, et hårcelleområdes frekvensbånd, hvor det tilsvarende frekvensbånds høretærskel, der er valgt fra hårcelleområdebillederne (300), er højere end en forudindstillet referenceværdi som målfrekvensbåndet, der svarer til det beskadigede hårcelleområde; og

(c) udlæsning med en stimuleringsbehandlingssektion af hårcellestimuleringsapparatet, et stimulerende akustisk signal til målfrekvensbåndet

med en forudindstillet intensitet til at stimulere det beskadigede hårcelleområde, hvor den forudindstillede intensitet er ca. 3 dB til 20 dB højere end det beskadigede hårcelleområdes høretærskel, hvor det stimulerende akustiske signal er mindst en amplitudemoduleret tone, en frekvensmoduleret tone, en pulstone, en vedvarende tone og amplitudemoduleret smalbåndsstøj eller en kombination af tonerne og støjen.

2. Registreringsmediet af krav 1, der består af kommandoer i tilfælde af, at adskillige hårcelleområder er beskadigede, får computeren til trinvist at udføre (b) en bestemmelse af et frekvensbåndområde, der svarer til hårcelleområder, der vedvarende findes blandt de beskadigede hårcelleområder som målfrekvensbåndet.

3. Registreringsmediet af krav 1, der består af kommandoer til at aktivere computeren, hvis der bestemmes flere målfrekvensbånd, at de tilsvarende akustiske signaler udlæses i rækkefølgen for beskadigelsesgraden eller vilkårligt i trin (c).

4. Registreringsmediet af krav 1, hvor registreringsmediet, i tilfælde af at der bestemmes flere målfrekvensbånd, omfatter kommandoer til at få computeren til at udføre en metode, hvor trin (c) samtidig udlæser de akustiske signaler, der svarer til målfrekvensbåndene.

5. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode, hvor k'et er et positivt heltal mellem 3 og 24.

6. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode, hvor trinnet udføres yderligere:

(d) udlæsning af hårcelleområdebilledet, der svarer til det bestemte målfrekvensbånd, hvor det udlæste hårcelleområde visualiseres.

7. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode med yderligere udførelse:

- udlæsning af hårcelleområdebilledet, der svarer til frekvensbåndet for en amplitudemoduleret tone, hvis typen af det akustiske signal er den amplitudemodulerede tone, hvor amplitudevariationen af den amplitudemodulerede tone visualiseres på hårcelleområdebilledet.

8. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få

computeren til at udføre en metode med yderligere udførelse:

- udlæsning af hårcelleområdebilledet, der svarer til frekvensbåndet for en frekvensmoduleret tone, hvis typen af det akustiske signal er den frekvensmodulerede tone, hvor frekvensvariationen af den frekvensmodulerede tone visualiseres på hårcelleområdebilledet.

9. Registreringsmediet af krav 8, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode, hvor den frekvensmodulerede tone har en opløsning på mindre end 1/3 oktav.

10. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode med yderligere udførelse:

- udlæsning af hårcelleområdebilledet, der svarer til det akustiske signals frekvensbånd, hvis typen af det akustiske signal er den vedvarende tone eller pulstonen, hvor det registreres gennem hårcelleområdebilledet, at det akustiske signal svarer til mindst den vedvarende tone eller pulstonen.

11. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode, hvor hårcelleområdebilledet udlæses med en anden farve eller størrelse afhængigt af omfanget af forbedring af høreevne.

12. Registreringsmediet af krav 1, hvor registreringsmediet består af kommandoer til at få computeren til at udføre en metode med yderligere udførelse:

- udlæsning af en cochlear-modelgrænseflade, der omfatter hårcelleområdebilleder (300) delt med 1/k oktavopløsning, hvor k'et er et positivt heltal over 2;
- udlæsning af det akustiske signal i et frekvensbånd, der svarer til mindst et område valgt fra ovenstående hårcelleområdebilleder; og
- registrering af beskadiget hårcelleområde på basis af brugerens respons på det udlæste akustiske signal.

DRAWINGS

FIGURE

FIG. 1

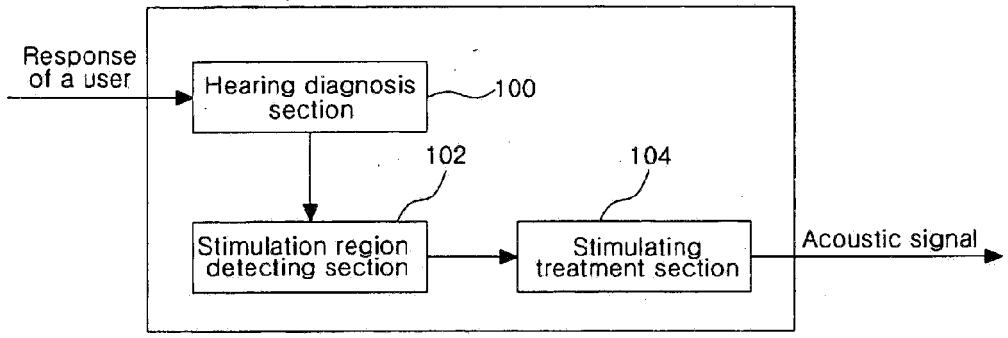


FIG. 2

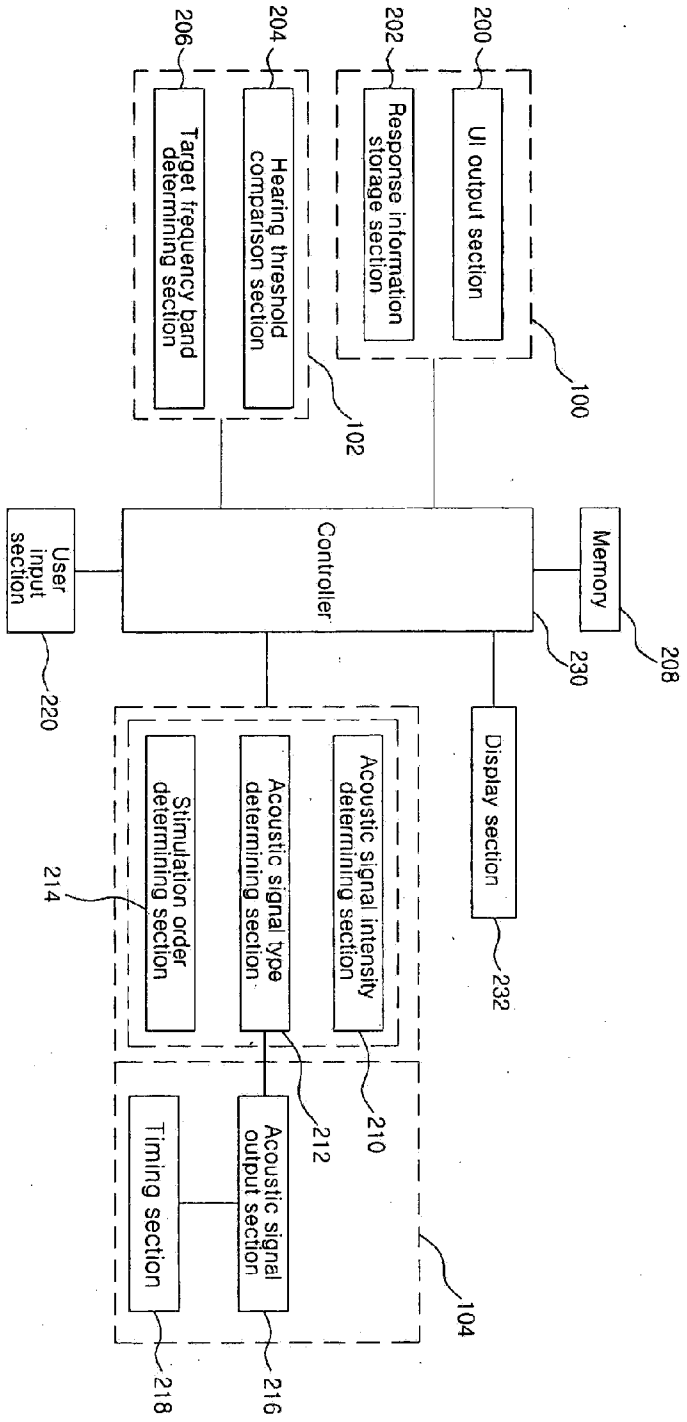

200
UI output section
202
Response information storage section
204
Hearing threshold comparison section
206
Target frequency band determining section
100
102
Controller
User input section
220
Memory
208
230
Display section
232
Acoustic signal intensity determining section
210
Acoustic signal type determining section
212
Stimulation order determining section
214
Acoustic signal output section
216
Timing section
218
104

FIG. 3

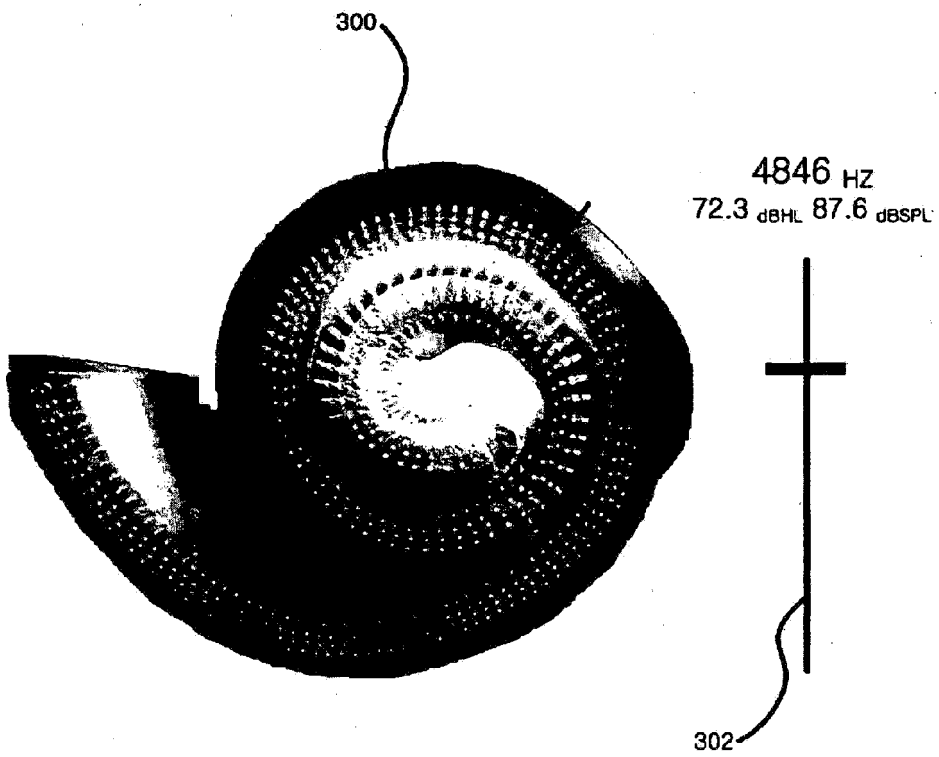


FIG. 4

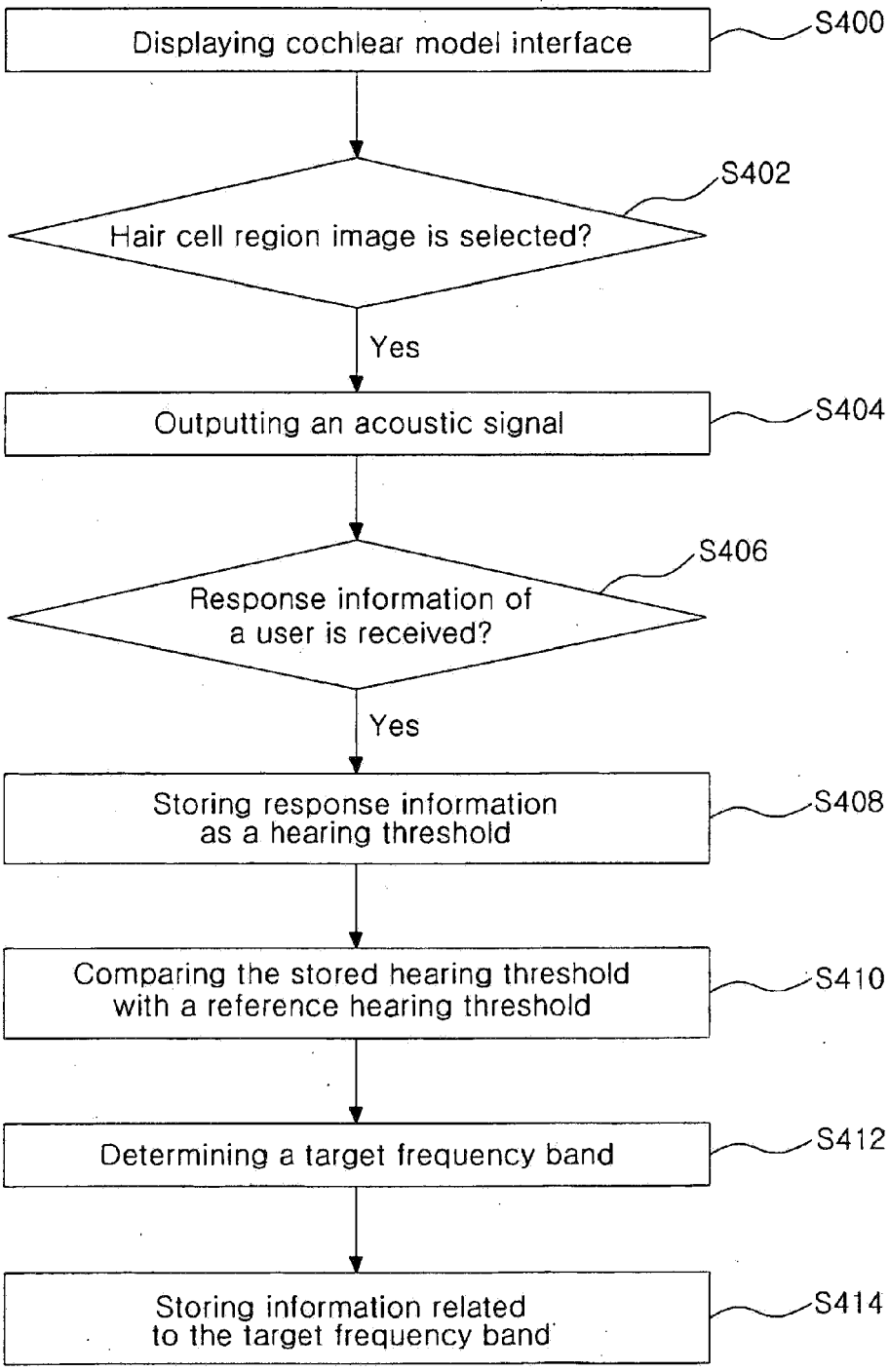

Displaying cochlear model interface
S400
Hair cell region image is selected?
S402
Yes
Outputting an acoustic signal
S404
Response information of a user is received?
S406
Yes
Storing response information as a hearing threshold
S408
Comparing the stored hearing threshold with a reference hearing threshold
S410
Determining a target frequency band
S412
Storing information related to the target frequency band
S414

FIG. 5

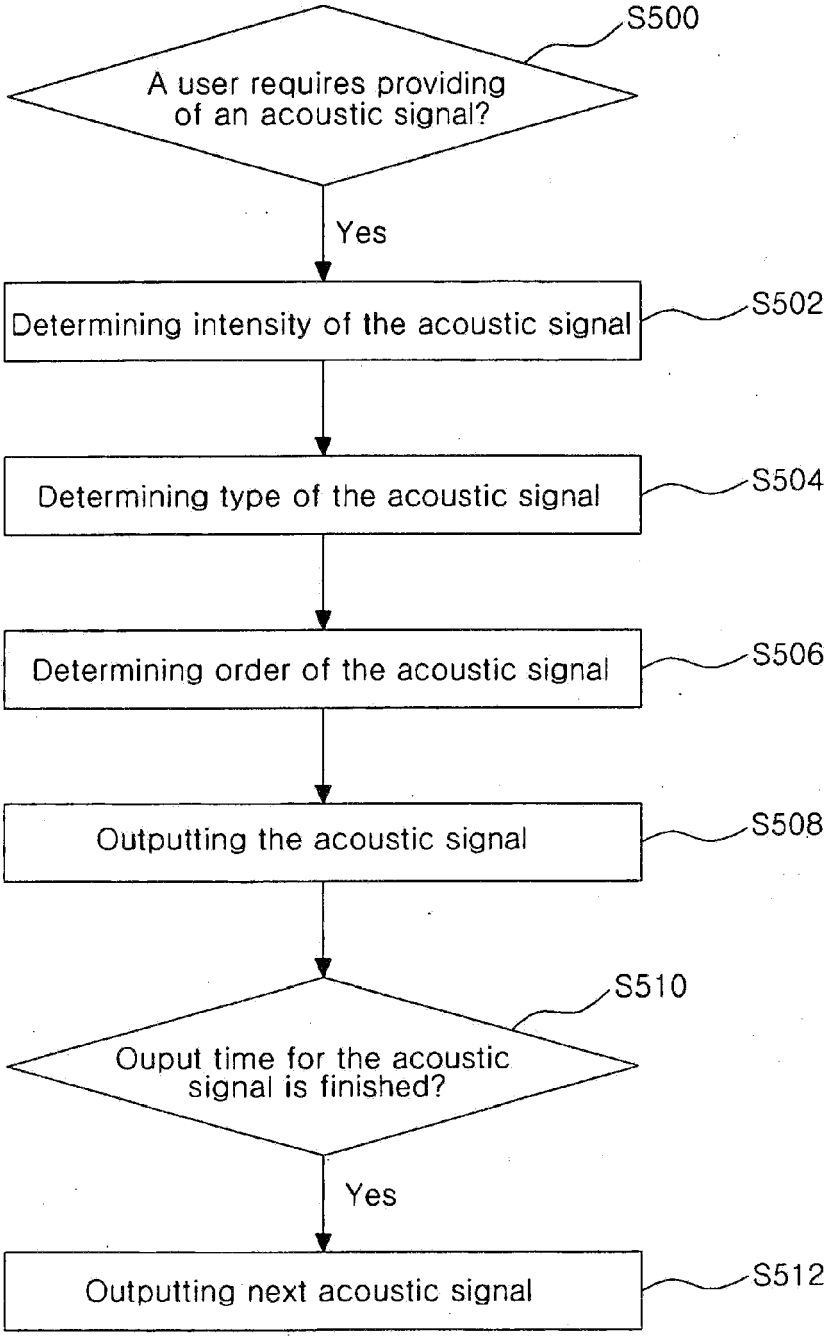

S500
A user requires providing of an acoustic signal?
Yes
Determining intensity of the acoustic signal
S502
Determining type of the acoustic signal
S504
Determining order of the acoustic signal
S506
Outputting the acoustic signal
S508
S510
Ouput time for the acoustic signal is finished?
Yes
Outputting next acoustic signal
S512

FIG. 6

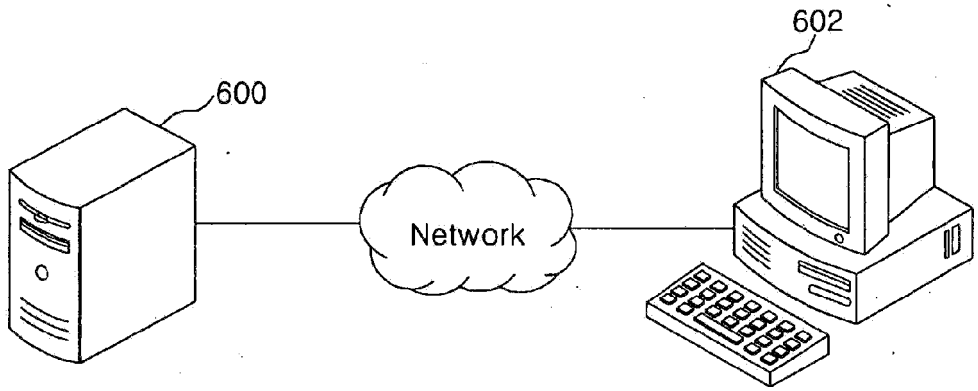

602
600
Network

FIG. 7

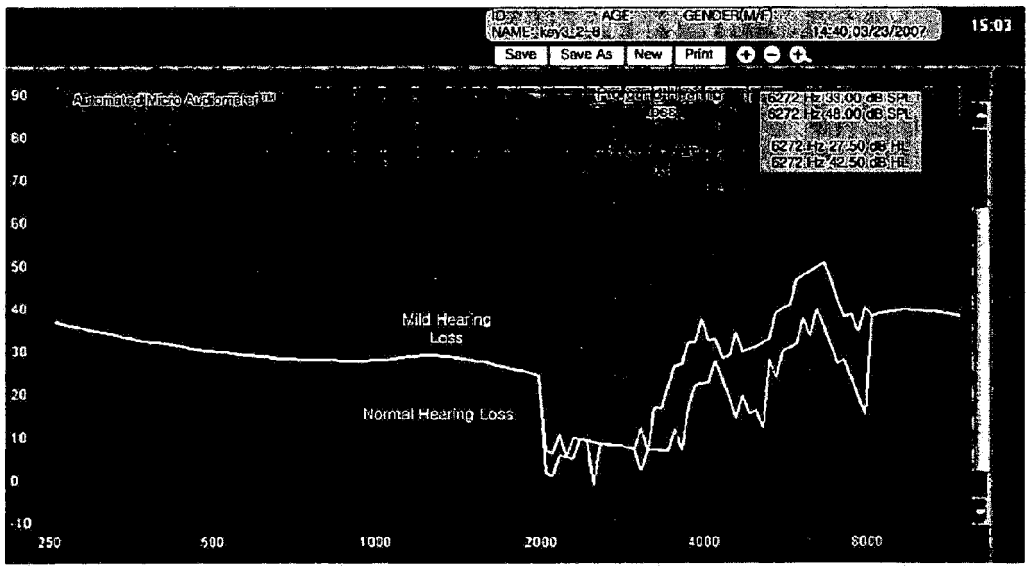

Save
Save As
New
Print
15:03
Automated Micro Audiometer™
90
80
70
60
50
40
30
20
10
0
-10
250
500
1000
2000
4000
8000
Mild Hearing Loss
Normal Hearing Loss

FIG. 8

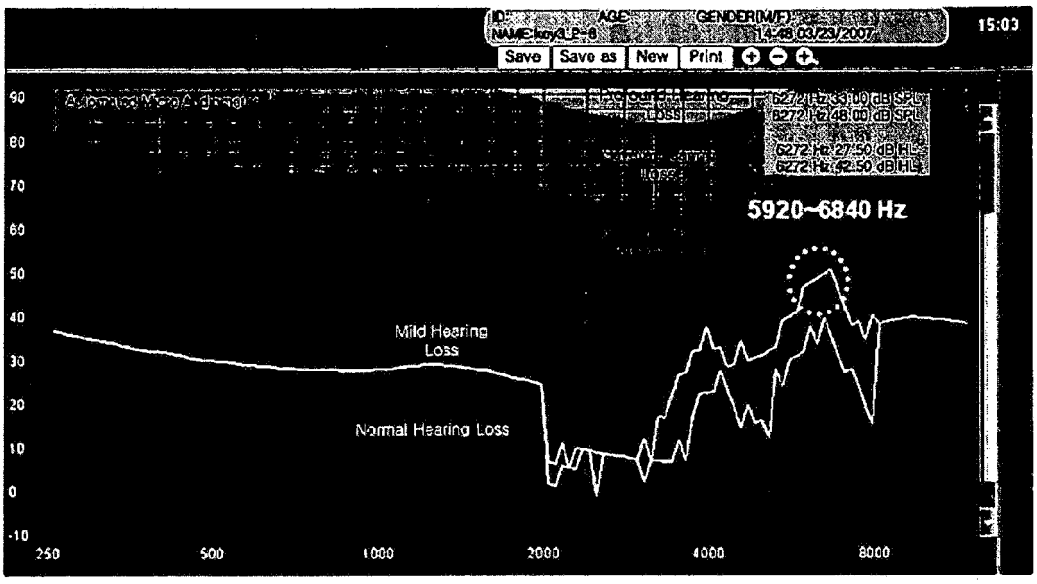

Save
Save as
New
Print
15:03
5920~6840 Hz
Mild Hearing Loss
Normal Hearing Loss
90
80
70
60
50
40
30
20
10
0
-10
250
500
1000
2000
4000
8000

FIG. 9

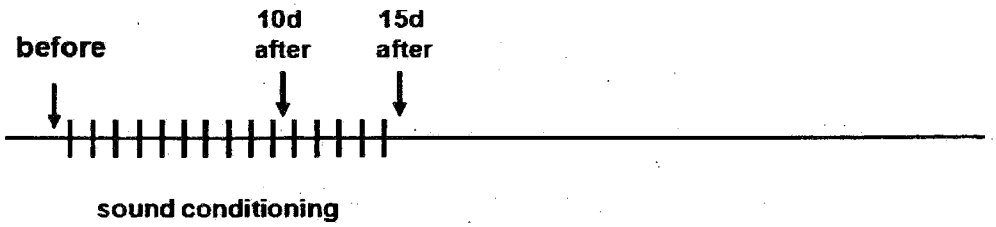

before
10d after
15d after
sound conditioning

FIG. 10

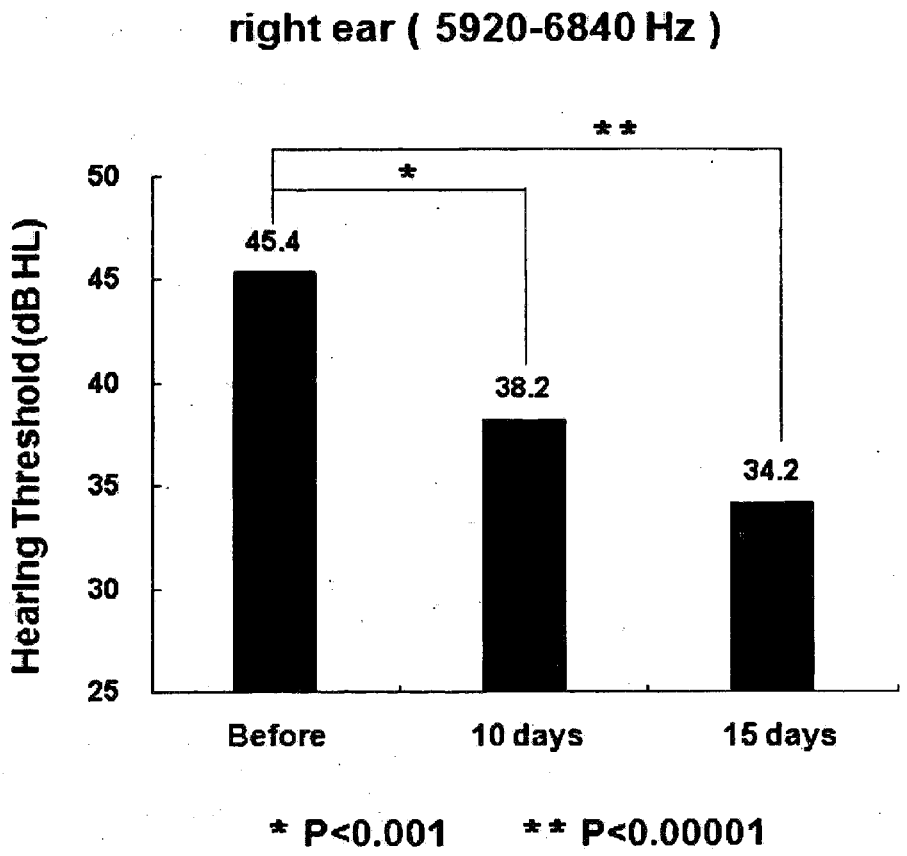

right ear (5920-6840 Hz)
Hearing Threshold(dB HL)
50
45
40
35
30
25
45.4
38.2
34.2
*
**
Before
10 days
15 days
* P<0.001
** P<0.00001

FIG. 11

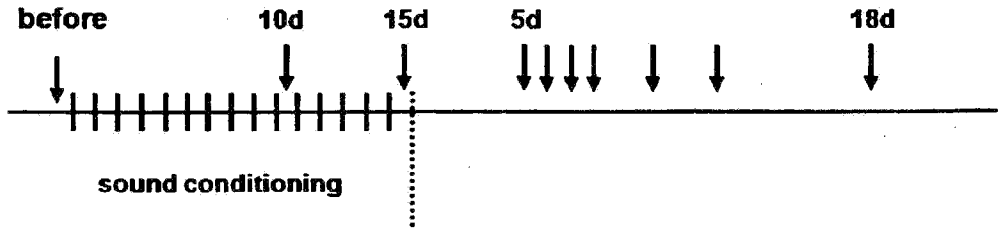
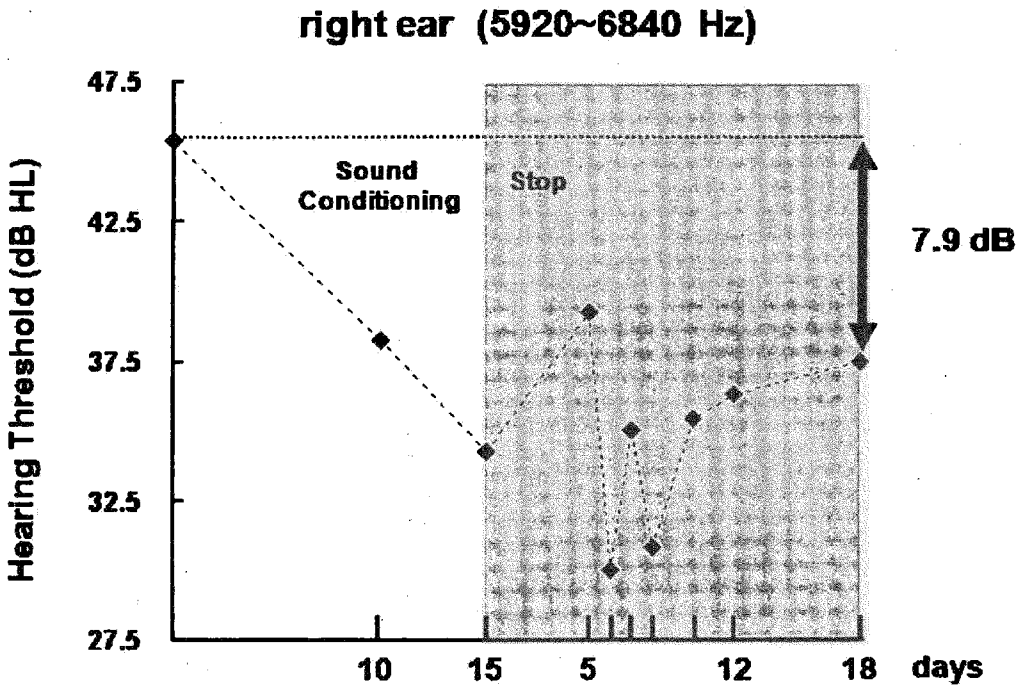

before
10d
15d
5d
18d
sound conditioning

FIG. 12


right ear (5920~6840 Hz)
Hearing Threshold (dB HL)
47.5
42.5
37.5
32.5
27.5
Sound Conditioning
Stop
7.9 dB
10
15
5
12
18
days