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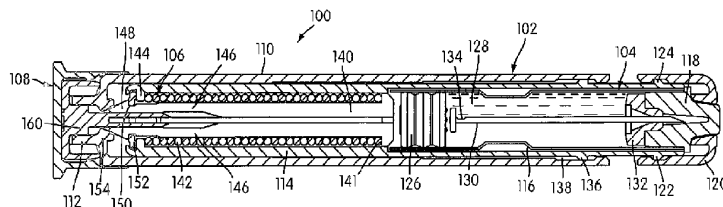
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(54) Title: AUTOMATIC INJECTOR WITH ANTI-CORING NEEDLE



(57) Abstract: The automatic injector (100) comprises a cartridge (104) adapted to contain a charge of medicament, a seal structure (118) disposed toward a forward end of the cartridge, a plunger (126) normally disposed in a generally rearward end of the cartridge and movable through the cartridge toward a generally forward end thereof in response to an actuating procedure. The movable plunger rearwardly confines the medicament within the cartridge. A needle (130) normally disposed in communication with the medicament container provides a passage in which the medicament is released into an individual's flesh in response to an actuating procedure projecting the needle into the flesh of the individual. The cartridge having an increased friction region (215) so as to slow the motion of the plunger when the forward end of the needle travels through the seal in order to eliminate coring.

**AUTOMATIC INJECTOR WITH ANTI-CORING NEEDLE****CROSS REFERENCE TO RELATED APPLICATIONS**

- 5        This application claims priority from U.S. Patent Application Serial No. 09/985466, filed November 2, 2001, the disclosure of which are incorporated herein in their entirety by reference.

**BACKGROUND**

## 10    1.    Field of Invention

The present invention relates to automatic injectors, and more particularly, to automatic injectors that reduce the likelihood of coring a sealing member.

## 2.    Discussion of Related Art

- 15        Automatic injectors are known. Basically an automatic injector is a device for enabling an individual to self-administer, or administer to another, a dosage of a liquid medicament. An advantage of automatic injectors is that they contain a measured dosage of a liquid medicament in a sealed sterile condition capable of storage in such condition for an extensive period of non-use, during which period immediate injection  
20        of the stored dosage may be accomplished at any time under severe emergency conditions.

- Another advantage of automatic injectors is the administration of the self-contained dosage of liquid medicament is accomplished without the necessity of the user initially seeing the hypodermic needle through which the liquid medicament is  
25        injected or of manually penetrating such visible needle into the user's or another person's tissue.

[0003] As stated above, automatic injectors are particularly suited for use under emergency conditions. For example many tens of millions of such automatic injectors have been manufactured and sold containing nerve gas  
5 antidotes for use under emergency chemical warfare conditions. Typical units which have been utilized for this purpose are disclosed in U.S. Pat. Nos 2,832,339, 3,882,863, and 4,031,893. In addition units of this type have been manufactured and used in administering anti-arrhythmic medicaments under emergency conditions relating to heart attack medical situations. The use of an  
10 auto injector has also been proposed to provide other medicaments useful in treating heart attack symptoms such as clot selective thrombolytic agents (for example, tPA) and related medicaments. See for example, U.S. Pat Nos 4,689,042, 4,755,169, and 4,795,433. In addition, automatic injectors have been widely marketed containing a dosage of epinephrine as an antidote for  
15 counteracting severe allergic reactions, as for example, to bee stings, and the like.

[0004] In all of these instances, the auto-injector is specifically structured so that in its normal operation the needle extends into the tissue of  
20 the individual and a specified amount of liquid medicament stored in a cartridge within the injector is injected into the tissue of the individual.

[0005] The hypodermic needle of an autoinjector has a forward end adapted to penetrate the clothing and flesh of an individual and a rearward end  
25 adapted to communicate with a liquid medicament source so that the medicament is permitted to flow from the source, through the central longitudinal bore or lumen in the needle, and into the flesh of the individual. In some embodiments, the needle is contained inside the cartridge containing the liquid medicament. For example one application exists in the field of  
30 automatic injection devices, wherein the liquid medicament is sealed within a

5 tubular container or cartridge, generally made of glass, plastic or metal, having a rubber seal closing off at the forward end and a rubber plunger at the rearward end. For example see U. S. Pat. No. 5,354, 286. During an injection operation, a stressed spring assembly is released moving a push rod against the plunger. The plunger pushes against the hub-end of the needle causing the needle to puncture the forward end seal of the cartridge and penetrates into the flesh of an individual. The liquid medicament is pushed at the same time through the needle, thus releasing the medicament into the individual's flesh.

10 In another type of automatic injector, the needle is connected to the forward end of the cartridge. See U. S. Pat No. 5,102, 393. During an injection operation, the needle is forced through a resilient seal at the forward end of the outer housing or through an elongated rubber sheath surrounding the needle. In either case the needle is kept sterile by a seal disposed toward a forward end of the housing while the injector is  
15 stored. After the needle punctures the seal or sheath, it then is forced into the flesh of the individual.

20 An issue that must be dealt with in each of the mentioned arrangements is that the forward end of the needle must perforate a rubber or other type of seal, and it is possible for the forward end of the needle to core out or dislodge a small particle of material from the seal and potentially block the needle orifice/lumen or be forced into the individual's flesh.

25 A reference herein to a patent document or other matter which is given as prior art is not to be taken as an admission that that document or matter was known or that the information it contains was part of the common general knowledge as at the priority date of any of the claims.

30 Throughout the description and the claims of this specification the word "comprise" and variations of the word, such as "comprising" and "comprises" is not intended to exclude other additives, components, integers or steps.

## SUMMARY OF INVENTION

5 To alleviate at least one of these problems and others, it is proposed to provide  
an automatic injector in which the amount of coring by the needle is substantially  
reduced or eliminated.

10 Therefore, in one embodiment of the present invention is to provide an automatic  
injector that comprises: a housing; a seal structure disposed toward a forward end of  
the housing; a cartridge contained within the housing; a charge of medicament  
contained in the cartridge; a plunger normally disposed in a generally rearward end of  
the cartridge and movable through the cartridge toward a generally forward end thereof  
15 in response to an actuating procedure. The movable plunger rearwardly confines said  
medicament within said cartridge. A needle is normally disposed within the housing,  
the needle being projectable from a forward end of said housing through said seal  
structure. The needle is communicable with the medicament so that movement of the  
plunger through the cartridge forces the medicament through the needle and into the  
20 flesh of an individual, in response to the predetermined actuating procedure. A  
releasable energy source is releasable in response to the predetermined actuating  
procedure to project the needle from the forward end of the housing and slidingly drive  
the plunger through the cartridge in sealed relation to expel the medicament through  
the needle and into the flesh of an individual. The cartridge has an increased friction  
region so as to slow the motion of the plunger as the forward end of the needle travels  
through the seal.

25 In another embodiment, the needle carries a damping structure for reducing the  
rate of acceleration of the needle by the resistance created when said damping structure  
moves within said medicament.

30 In addition, the present invention is directed to several automatic injection  
devices comprising novel needle structures that reduce coring of an elastic, plastic or  
rubber based structure at the forward end of the injector.

In another embodiment, the present invention provides an automatic injector comprising:

- a housing having a rearward end and a forward end;
- a seal structure disposed toward the forward end of said housing;
- 5 a cartridge contained within said housing;
- a charge of medicament contained in said cartridge;
- a plunger normally disposed in a generally rearward end of said cartridge and movable through said cartridge toward a generally forward end thereof in response to an actuating procedure, said movable plunger rearwardly confining said medicament
- 10 within said cartridge;
- a needle normally disposed within said housing, said needle being projectable from the forward end of said housing through said seal structure, said needle being communicable with said medicament so that movement of said plunger through said cartridge forces said medicament through said needle and into the flesh of an
- 15 individual in response to said predetermined actuating procedure; and
- a releasable energy source releasable in response to said predetermined actuating procedure to project said needle from the forward end of the housing and slidably drive said plunger through said cartridge in sealed relation to expel said medicament through said needle and into the flesh of an individual, said cartridge having an
- 20 increased friction region for engaging said plunger so as to temporarily slow the motion of said plunger as said plunger travels through the cartridge when the forward end of the needle travels through said seal.

In another embodiment, the present invention provides an automatic injector

- 25 comprising:
- a housing having a rearward end and a forward end;
- a seal structure disposed toward the forward end of said housing;
- a cartridge contained within said housing;
- a charge of medicament contained in said cartridge;
- 30 a plunger normally disposed in a generally rearward end of said cartridge and movable through said cartridge toward a generally forward end thereof in response to an actuating procedure, said movable plunger rearwardly confining said medicament within said cartridge;

5 a needle normally disposed within said housing, said needle being projectable from the forward end of said housing through said seal structure, said needle being communicable with said medicament so that movement of said plunger through said cartridge forces said medicament through said needle and into the flesh of an individual in response to said predetermined actuating procedure; said needle having a longitudinal axis and comprising:

10 a hollow rigid tubing having a cylindrical wall defining a longitudinal passage therethrough, wherein said longitudinal passage extends parallel to said longitudinal axis substantially along the entire length of said passage, said cylindrical wall including opposing first and second wall portions, said first wall portion having a forward tip portion terminating in a forward end tip, said second wall portion terminating at a position rearwardly spaced from said end tip, said forward tip portion being bent in a single direction in a manner to shield the entire cross-section of said longitudinal passage, said forward tip portion bent at an angle approximately between 15 51 degrees and 100 degrees; said angle defined as the angle between a tangent to a curvature of an outer surface at said forward end tip and the longitudinal axis of said needle;

20 a releasable energy source releasable in response to said predetermined actuating procedure to project said needle from the forward end of the housing and slidingly drive said plunger through said cartridge in sealed relation to expel said medicament through said needle and into the flesh of an individual.

25 In another embodiment, the present invention provides a method for injecting a medicament with an automatic injector, which injector comprises a housing, a seal structure disposed toward a forward end of said housing, a cartridge contained within said housing, a charge of medicament contained in said cartridge, a plunger movable through said cartridge toward a generally forward end thereof in response to an actuating procedure, said movable plunger rearwardly confining said medicament within said cartridge, a needle normally disposed within said housing, said needle being projectable from the forward end of said housing through said seal structure, said needle being communicable with said medicament so that movement of said plunger through said cartridge forces said medicament through said needle and into the flesh of an individual in response to said predetermined actuating procedure, a releasable

energy source releasable in response to said predetermined actuating procedure to project said needle from the forward end of the housing and slidably drive said plunger through said cartridge in sealed relation to expel said medicament through said needle and into the flesh of an individual;

- 5       said method comprising:
- releasing said energy source;
- accelerating said needle forwardly within said housing;
- reducing the rate of acceleration of said needle prior to said needle penetrating said seal; and
- 10       expelling said medicament through said needle.

          In another embodiment, the present invention provides a method for injecting a medicament with an automatic injector, which injector comprises a housing, a seal structure disposed toward a forward end of said housing, a cartridge contained within

15       said housing, a charge of medicament contained in said cartridge, a plunger movable through said cartridge toward a generally forward end thereof in response to an actuating procedure, said movable plunger rearwardly confining said medicament within said cartridge, a needle normally disposed within said housing, said needle being projectable from the forward end of said housing through said seal structure, said

20       needle being communicable with said medicament so that movement of said plunger through said cartridge forces said medicament through said needle and into the flesh of an individual in response to said predetermined actuating procedure, a releasable energy source releasable in response to said predetermined actuating procedure to project said needle from the forward end of the housing and slidably drive said

25       plunger through said cartridge in sealed relation to expel said medicament through said needle and into the flesh of an individual;

- said method comprising:
- releasing said energy source;
- moving said needle forwardly within said housing at a speed of less
- 30       than 680 inches/s as said needle penetrates said seal; and
- expelling said medicament through said needle.

## BRIEF DESCRIPTION OF THE DRAWINGS

5       These and other aspects and advantages of the invention will become more  
apparent and more readily appreciated from the following detailed description of the  
presently preferred exemplary embodiments of the invention, taken in conjunction with  
the accompanying drawings, of which:

10       Figure 1 is a longitudinal sectional view of an automatic injector according to an  
embodiment of the present invention;

Figure 2 is a longitudinal sectional view of a cartridge showing the friction  
region according to an embodiment of the present invention;

Figure 3 is a longitudinal sectional view of the cartridge showing the friction  
region according to an alternative embodiment of the present invention;

15       Figure 4 is a graph showing the force versus distance of travel of plunger in a  
configuration without an increased friction region, as will be described hereinafter;

Figure 5 is a graph showing the force versus distance of travel of plunger in a  
configuration when using embodiment illustrated in Figure 3;

20       Figure 6 is a graph showing the force versus distance of travel of plunger in a  
configuration when using embodiment illustrated in Figure 2;

Figure 7 is a graph showing the percentage of coring versus the inside diameter  
measured at an increased friction region, as will be described hereinafter;

Figure 8 is a graph showing the core length versus the inside diameter measured  
at an increased friction region, as will be described hereinafter;

25       Figure 9 is an enlarged view of a straight tip showing the point and the heel of  
the needle.

[0022] Figure 10 is a longitudinal sectional view of the hypodermic needle as installed in a cartridge according to another embodiment of the present invention; the hypodermic needle is shown having a curved tip;

[0023] Figure 11A is an enlargement of the tip of the needle according to embodiment illustrated in Figure 10 having curved "C" tip;

[0024] Figure 11B is an enlargement frontal view of the pointed tip of the needle;

[0025] Figure 12 is a longitudinal expanded sectional view of the forward end of the needle showing the interaction of the seal material with a curved tip needle having a regular/thinner wall thickness;

[0026] Figure 13 is a longitudinal expanded sectional view of the forward end of the needle showing the interaction of the seal material with a needle having a heavy/thicker wall thickness;

[0027] Figure 14 is a longitudinal expanded sectional view of the forward end of the needle showing the curvature tolerance limits;

[0028] Figure 15 is a longitudinal expanded sectional view of the forward end of the needle showing the front-ground geometry;

[0029] Figure 16 is a sectional transversal view of the forward end of the needle showing the front-ground geometry;

[0030] Figure 17 is a longitudinal expanded sectional view of the forward end of the needle showing the back-ground geometry;

[0031] Figure 18 is a sectional transversal view of the forward end of the needle showing the back-ground geometry;

[0032] Figure 19 shows the consecutive transversal sectional views of the forward end of the needle illustrating the back-ground geometry;

[0033] Figure 20 shows consecutive transversal sectional views of the forward end of the needle illustrating the front-ground geometry;

[0034] Figure 21 is a longitudinal view of the forward end of the needle according to an alternative embodiment of the present invention where Parylene coating is applied to the needle;

[0035] Figure 22 is a longitudinal expanded view of the heel of needle according to embodiment illustrated in Figure 21. The heel is shown uniformly coated with a conformal coating;

5 [0036] Figure 23 is a graph showing the percentage of coring and the coring mean length versus the coating thickness as applied in embodiment illustrated in Figure 22; and

[0037] Figure 24 is a longitudinal sectional view of an automatic injector according to another embodiment of the present invention.

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#### DETAILED DESCRIPTION OF PREFERRED EMBODIMENT

[0038] In the following description, for purposes of explanation and not limitation, specific details are set forth such as particular shapes and materials, mechanical components, techniques, etc. in order to facilitate a thorough understanding of the present invention. However, the invention may be practiced in other embodiments that depart from these specific details. The terms "damping structure", "friction area", "speed bump" and "narrowed diameter portion" are used interchangeably in this description to illustrate a feature that is used as a way to reduce the rate of acceleration thus decrease the speed at which the hypodermic needle punctures or pierces the forward seal in comparison with prior art auto-injectors. Also, for the purpose of this disclosure, the portions of the injector on the right side of Figure 1 (on the needle extension end) will be considered the front end, while the left side or activation end will be considered the rear end.

[0039] Referring, more particularly, to the drawings in detail, there is shown in Figure 1 an automatic injector 100. The automatic injector 100 includes a tubular housing 102, a medicament cartridge assembly 104, within the forward end portion of the housing assembly 102, and a releasable energy

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source 106 which is releasable in response to a predetermined actuating procedure as will be described in detail in the following paragraphs. While the releasable energy source can be any type of assembly which effectuates an injection operation, such as a compressed gas assembly as disclosed in U.S. Patent No. 4,518,384, it is preferred that the releasable energy source be a stressed spring assembly, as generally indicated at 106. The stressed spring assembly is disposed within the rearward end portion of the housing assembly 102 in operative relation with the medicament cartridge assembly 104. A releasable end safety cap 108 positioned at the rear of the housing assembly 102 is in operative relation with the stressed spring assembly 106.

[0040] The housing assembly 102, medicament cartridge assembly 104, and stress spring assembly 106 are generally constructed in accordance with the teaching of U.S. Pat. No. 2,832,339, hereby incorporated by reference. As shown in Figure 1, the housing assembly 102 includes a cylindrical outer housing member 110 having a centrally apertured cylindrical rear wall portion 112 of reduced diameter on which the safety end cap 108 is mounted. The housing assembly 102 also includes an inner cylindrical housing member 114 within the housing member 110 within which is mounted the medicament cartridge assembly 104 and the stressed spring assembly 106. The forward portion of the inner housing member 114 is formed with a counterbore for receiving therein a cylindrical dosage container or cartridge 116 of the medicament cartridge assembly 104. The cartridge of the present invention is preferably made of metallic materials such as, but not limited to, stainless steel and aluminum. Other materials, such as plastic materials (eg., polypropylene) or glass are also within the scope of the present invention.

[0041] The forward end of the container or cartridge 116 is closed by a stopper or seal 118, preferably, of suitable rubber or compliant plastic material. The cartridge assembly 104 is retained in closing relation with the

forward end of the inner housing member 114 by a housing end cap member 120 of molded plastic material. The cap 120 is preferably retained on the inner housing member 114 by inter-engagement of a pair of ridges 122 formed on the exterior periphery of the tubular member 114 with an annular groove 124  
5 formed on the interior periphery of the cap member 120. The rearward end of the cartridge 116 is closed by a rubber or plastic plunger 126 which is slidably, sealingly engaged with the inner surface of cartridge 116 so as to enclose within the cartridge a dosage 128 of a liquid medicament.

10 [0042] A hypodermic needle 130 is disposed within the cartridge 116. It thus can be appreciated that the cartridge assembly 104 includes cartridge 116, seal 118, needle 130 and disc 132. As can be discerned from FIG. 1, needle 130 is normally stored in contact with the medicament 128. However, in the broadest aspects of the present invention, it can be appreciated that  
15 needle 130 can be disposed in a separate chamber (either evacuated or filled with a preferably inert gas) forwardly of the medicament 128 (for example, see our U.S. Pat. No. 5,085,642 and 5,102,393), so long as the needle is somehow communicable with the medicament in a manner which permits the medicament to travel through the needle and into the flesh of an individual.  
20 The needle can also be disposed in contact with one of two medicaments, which are normally stored separately within the injector and then either mixed within the injector prior to an injection (e.g. see U.S. Pat. No. 5,041,088) or injected separately one after the other (see U.S. Pat. No. 5,092,843). The hypodermic needle 130 is preferably made from stainless steel.

25 [0043] In the present embodiment, the needle 130 has its pointed end disposed within a recess formed in the seal 118. A disc 132 of plastic is disposed within the forward end of the cartridge 116 in surrounding, securing and guiding relation with the hypodermic needle 130 and in abutting  
30 engagement with the seal 118. The disc 132 serves to releasably hold the

needle in its storage position to provide peripheral centering therefore during the dosage injecting stroke of the plunger 126. The rearward end of the hypodermic needle 130 is enlarged for engagement by the plunger and has a slot 134 formed in its side wall adjacent the enlarged end for communicating the dosage 128 with the hollow interior of the hypodermic needle 130 when the plunger 126 is in engagement therewith. The inner housing member 114 is mounted within the outer housing member 110 for limited reciprocating movement as determined by a pair of ridges 136 formed on the exterior periphery of the tubular inner housing member 114 at a position spaced rearwardly from the pair of ridges 122. The pair of ridges 136 is adapted to engage with an elongated annular groove 138 formed on the interior periphery of the outer housing member 110.

[0044] The stressed spring assembly 106 includes a normally compressed but releasable coil spring 142 and an elongated collet member 140. The collet member is disposed within the rearward portion of the housing member 114 and has its forward end disposed adjacent to the plunger 126. The forward end of the collet member 140 has a flange 141 configured to engage the forward end of the stressed coil spring 142, which surrounds the central portion of the elongated collet member 140. The collet 140 has its rearward end engaged with a locking ring 152 sitting on an annular end flange 144 formed integrally on the rearward end of the inner housing member 114.

[0045] The rearward end of the elongated collet member 140 are split to provide a plurality (e.g., four) flexible spring fingers 146, the rearward extremities of which are formed with rearwardly and outwardly facing cam releasing surfaces 148. Extending inwardly from the rearward end of each cam surface 148 is locking shoulder 150 adapted to engage a locking ring 152 seated on the rear surface of flange 144. The forward portion of the apertured cylindrical wall portion 112 is formed with a complementary cam surface 154,

which is disposed in engagement with the cam surfaces 148 so as to effect a laterally inward movement of the spring fingers 146 toward one another to disengage locking shoulders 150 from locking ring 152 in response to a relative forward actuating movement of the outer housing member 110 with respect to the inner housing member 114. This inward action of the spring fingers 146 is permitted only after the safety cap 108 is removed, as will be described.

[0046] The operation of the injector will now be described. In the first step of operation, releasable end cap 108 is removed from the injector 100. This removal is accomplished simply by gripping the exterior periphery of the end cap 108 and moving it rearwardly while gripping and holding the outer housing member 110. The cap member 108 carries with it a safety pin portion 160. With the safety pin portion 160 removed from its safety position, which normally prevents the laterally inward movement of the spring fingers 146, the user can now complete the operation by moving the forward cap member 120 into contact with the tissue of a person to be injected. By applying a continued forward force on the exterior periphery of the outer housing member 110, cam surfaces 154 thereof are moved forwardly. This forward movement in cooperation with the cam surfaces 148 on the spring fingers 146 causes the locking surfaces 150 of the latter to move inwardly off of the locking ring 152, thus releasing the stressed spring 142. The spring 142 acts through the collet member 140 to move the same forwardly which has the effect of moving the plunger 126 with it. As the plunger moves forwardly, it carries with it the needle 130. The pointed forward end of the needle pierces through the seal 118 and into the tissue of the patient. At the same time, the dosage 128 of liquid medicament within the cartridge 116 is caused to move inwardly into the slot 134 of the needle and outwardly of the pointed forward end thereof as the same moves into the tissue of the user.

30

[0047] Referring more particularly to Figure 2A, describing in more detail the cartridge assembly 104. The hypodermic needle 202 comprises an elongated tube, generally cylindrical terminated at the rearward end by hub 206. The forward end of the needle has a pointed shape 208, shown in more detail in enlarged Figure 2B. The needle 202 is maintained along a longitudinal axis X with holder 210. Needle 202 is shown housed inside cartridge 212, containing a liquid medicament. However as stated previously needle 202 need not be inside cartridge 212 but can be arranged to be outside the medicament cartridge. The forward end of cartridge 212 is terminated by seal 214 to keep the liquid medicament from leaking, shown in more detail on Figure 2B. The pointed end 208 of needle 202 is oriented toward seal 214. Therefore, initially the needle 202 is disposed between plunger 204 and seal 214. The plunger is shown in this figure as a one piece material, however it is understood that the plunger can be made of a plurality of pieces with various ductile constants such as a harder piece and a softer piece of rubber.

[0048] Seal 214 is made of a flexible material, such as but not limited to, rubber. It is known that polymers behave in a ductile manner when strained at low speed and behave in a brittle manner when strained at high speed.

[0049] In order to substantially reduce or eliminate coring, the needle 202 is arranged to penetrate in a "gentle" manner into the rubber seal 214 by reducing the thrust of the needle. Cartridge 104 has a friction region 215 for slowing the motion of plunger 204 thus reducing the rate of acceleration of needle 202 when perforating seal 214. The acceleration rate is reduced so that the speed of the needle is less than 680 inches/s when the needle pierces the seal. The reduction in acceleration rate is intended specifically to reduce the speed to a level at which coring will not occur. Preferably, the speed at which the seal is pierced is also greater than 150 inches/s so that the injection operation is not delayed more than what is desirable. The friction region in

this embodiment is a narrowed diameter portion or localized narrowed diameter portion 222 in the wall 224 of cartridge 212. The narrowed diameter portion 222 also referred to as speed bump is arranged between seal 214 and plunger 204. The narrowed diameter portion 222 is arranged and configured to  
5 reduce acceleration of plunger 204, thus reducing the speed at which the needle 202 would otherwise travel when the needle tip 208 travels through seal 214. The narrowed diameter portion 222 is created on the wall of the cartridge 212 with a pressure forming method, for example with a clamshell die. The die or a rolling process can be used to imprint a selected shape to the  
10 stainless wall of cartridge 212. For example cylindrical rounded narrowed diameter portion around the cylindrical wall of the cartridge can be imprinted.

[0050] The localized narrowed diameter portion 222 in the wall 224 of cartridge 212 acts as a "speed bump" by slowing down the motion of plunger  
15 204. Indeed, the narrowed diameter portion 222 increases the normal force between the plunger periphery and the wall 224 of cartridge 212, thus creating a frictional force counter to the plunger's movement. The narrowed diameter portion 222 increases the diametrical interference thereby increasing the friction and retarding plunger 204 movement. This slowed movement causes  
20 the needle 202 to strain the seal 214 in a more ductile mode, thus leading to a substantial reduction in coring.

[0051] The speed bump is arranged to be only effective along a partial length of the cartridge 212. This allows the plunger to receive the full spring  
25 force at the beginning of operation helping to overcome static friction between the plunger 204 and the cartridge 212. The speed bump then takes effect immediately prior to the front end of the needle contacts the seal 214. After the needle tip 208 completes its penetration of the seal 214, the speed bump disengages making the full spring force available to ensure completeness of  
30 the injection process.

[0052] The plunger 204 meets increased resistance when the plunger 204 reaches the narrowed diameter portion 222. Plunger 204 has a plurality of ribs 230 as shown in Figure 2C. Each time a rib 230 of the plunger 204  
5 encounters an edge of narrowed diameter portion 222 the friction force is increased thus leading to a net decrease in injection acceleration rate.

[0053] In another embodiment, illustrated in Figure 3A, the friction region 300 comprises a corrugated configuration comprising a plurality of  
10 projections 302, shown enlarged in Figure 3B, in order to multiply the interference with the plunger 304.

[0054] It is to be understood however, that friction region 300 can be any structure of the cartridge that slows plunger 304. While in the  
15 embodiments shown it is the wall of the cartridge itself that performs this function, it should be appreciated that the cartridge may employ a separate structure inserted therein. The plunger 304 meets increased resistance when the plunger's leading rib crosses the friction region leading edge. The rippled shape of friction region 300 illustrated in Figure 3 exchanges some of the  
20 aforementioned diameter decrease in the previous embodiment in exchange for a multitude of leading edges.

[0055] To demonstrate the effectiveness of the present invention in substantially reducing formation of cores, a series of tests are implemented  
25 and data is acquired.

[0056] Figure 4 shows the force-distance data profile of a standard cartridge-plunger. The curve 400 exhibits a high static friction spike 402 followed by a constant kinetic friction stage 404. Numerous tests are run to  
30 collect statistical data. The mean kinetic friction from the statistical data is

determined to be 0.54 lb. The nearly vertical spike 406 at the terminus represents bottoming of the plunger against the seal.

[0057] Figure 5 shows the force-distance data profile of a cartridge having corrugated portion and a plunger, as illustrated in Figure 3. The portion of travel in which the ripples are in effect is clearly visible on curve 500. The "spikiness" of data at the friction phase 502 is caused by the individual matings and separations of the individual ripples with plunger ribs. Similarly statistical data is acquired to allow calculation of the mean kinetic friction during the speed bump phase. The mean kinetic friction is determined to be 1.47 lb. The mean kinetic friction of the post speed bump phase, shown on Figure 5 as phase 504, is 0.52 lb.

[0058] Figure 6 shows the force-distance data profile 600 of a smooth speed bump and a plunger having three ribs, as illustrated in Figure 2. The three large consecutive spikes 602 are caused by the three ribs of the plunger entering the speed bump. The smaller spikes 604 occur as the plunger's ribs exit the speed bump. Similarly statistical data is acquired to allow calculation of the mean kinetic friction during the speed bump phase. The mean kinetic friction during the speed bump phase is determined to be 1.71 lb. The mean kinetic friction of the post-speed bump phase, shown on figure 6 as phase 606, is similar to the data described previously.

[0059] Data is also acquired to demonstrate that the introduction of the speed bump reduces coring. Figure 7 shows the coring frequency versus the inside diameter of the cartridge at the speed bump. The highest point on the curve corresponds to the inside diameter 0.298" of the cartridge without a speed bump. At this size (without a speed bump) approximately 70% of units tested produced cores. The lowest point on the curve corresponds to the

smooth (without ridges) speed bump in its intended diameter of 0.278".

Statistical data showed a population of less than 1% revealed coring.

5 [0060] In the case of a cartridge with a speed bump, a softer spring for pushing the plunger, may be used if desired to allow a smoother transition from the diameter of cartridge without the bump to the diameter of the cartridge at the bump.

10 [0061] In addition to coring frequency, the diameter of the particles generated by coring are also measured and reported in Figure 8. As seen in Figure 8, the dimension of the core (particle) decreases when the inside diameter of the cartridge at the speed bump decreases. Therefore, the speed bump has also an advantage in decreasing the size of the coring particles.

15 [0062] These tests are carried out for a straight tip needle such as shown in Figure 9 (which is a simplified view of the needle of Figure 3A). Needle tip 900 has generally a point 902 and a heel 904. As can be seen in the following embodiments the needle tip can have a curved shape instead of a straight shape as in Figure 9.

20 [0063] Figure 10 shows a longitudinal sectional view of the automatic injector with hypodermic needle according to another embodiment of the present invention. The hypodermic needle 1000 is shown having a curved tip 1002. As mentioned previously, and now illustrated in Figure 11A, the curved leading edge 1002 of needle 1000 having a C-tip configuration pushes the material of the seal 1004 far enough away from the heel 1100 to prevent intimate contact. The curved arrow 1102 indicates the direction of flow of seal material relative to the movement of the needle 1000. The arrow indicates in particular that the seal material flows around the curved tip 1002.

25

30 In other words, the curved tip 1002 acts as a shield for the orifice or lumen

1104 of needle 1000, by blocking the seal material 1004 from penetrating through the orifice 1104. The extent to which the needle tip is curved over the orifice influences seal coring frequency.

5       **[0064]** Figure 11B shows an enlargement frontal view of the pointed tip 1110 of the needle. The curved forward tip 1114 is shown completely shielding lumen 1112 thus protecting lumen 1112 of being in direct contact with the seal material as previously discussed. In other words, the bent tip 1114 shields the entire cross-section of the longitudinal passage in the needle.

10       **[0065]** Figure 12 shows the interaction of seal material 1200 with needle 1202 having a regular wall thickness, preferably between 0.0055 inch and 0.0065 inch. Figure 13 show the interaction of seal material 1300 with needle 1302 having a thicker wall (heavy wall) preferably between 0.0083  
15       inch and 0.0090 inch. In particular, Figure 13 illustrates that in the case of needle with heavy wall thickness 1302, the heel 1304 is further away from the seal material 1300, thus further reducing coring potential compared to needle with regular wall thickness 1202. Testing shows that in the eventuality cores are produced, cores are generally smaller when using heavy-wall needles  
20       versus regular wall needles of similar geometry.

**[0066]** Figure 14 shows the geometry of the C-tip needle 1400 with manufacturing limits for the hard C-tip geometry. The needle comprises a hollow rigid tubing 1401 having a cylindrical wall defining a longitudinal  
25       passage. The cylindrical wall includes first and second opposing wall portions. First wall portion is illustrated in this figure by longitudinal cross-section 1404 and second wall portion is illustrated in this figure by longitudinal cross-section 1406. The first wall portion 1404 has a forward tip portion 1408 terminating in a forward end tip 1410. The second wall  
30       portion 1406 terminating at a position 1412 rearwardly spaced from the end tip

1408. The forward tip portion 1408 is bent at angle 1414. Angle 1414 is defined as the angle between tangent 1416 to curvature of the outer surface at the end tip 1410 and the longitudinal axis 1418 of needle 1400. In one embodiment, the forward end tip 1410 terminates in a region defined by an imaginary forward extrapolation of the thickness of second wall 1406 defined by limits 1422 and 1424 which are intended to insure that the end tip 1410 is always deflected far enough to always shield the lumen or opening 1420, but not deflected so far to hinder the penetration or withdrawal of the needle (this applies equally to the embodiment of Figure 17). Other C-tip geometry is the soft C-tip needle where the tip is deflected such that it is aligned with the cannula centerline or longitudinal axis 1418. The soft C-tip geometry does not reduce coring as well as the hard C-tip geometry of needle 1400 of the present invention.
- 15           **[0067]** The hard C-tip needle is manufactured according to the following process: Two-meter length of tubes are bundled and are cut to the cannula blank length. The ends of the tubes are de-burred and the tubes cleaned. The tubes are then automatically fed and automatically taped onto 18 inch grinding fixtures. The tubes on the grinding fixtures are placed on a grinding machine where a primary grind facet is applied. The tubes are then inclined and rotated to grind a second facet and inclined and rotated again to grind a third facet. The second and third facets are preferably symmetrical to one another. The cannula needle tip are rolled over to produce the curved hard "C" tip. The cannula are de-burred again and an anti-coring micro-blast is applied to the heel. The micro-blast may alternately be applied before bending. The cannula are electro or chemically polished then cleaned, dried, passivated and inspected before packaging. The cannula are packaged with the points/tips oriented in the same direction and wrapped in non-shedding paper to be placed in a polyethylene bag and into a foam line carton for distribution.

[0068] All hypodermic needles have primary and secondary facets.

The secondary facets are called lancets. Figure 15 shows a sectional longitudinal view of a C-tip needle 1500. Lancets 1502 are shown in relation to the primary bevel 1504. A sectional transversal cut 16 of the tip 1508 is shown in Figure 16 with a front ground where the tip 1508 is ground from the inside as shown on transversal cut 1600. Figure 17 shows a sectional longitudinal view of a C-tip needle 1700. Lancets 1702 are shown in relation to the primary bevel 1704. A sectional transversal cut 18 of the tip 1708 is shown in Figure 18 with a back ground where the tip 1708 is ground from the outside as shown on transversal cut 1800. Back-ground lancets bring advantages to a C-tip needle. An advantage is that the angled lancets may serve to further direct seal material away from the lumen. Another advantage is that the effectively narrower thus sharper leading edge may cut through clothing and skin or tissue more easily. The use of heavy-wall cannulas provides more wall thickness allowing a better optimization of the geometry of the back-ground lancets.

[0069] Figure 19 shows the consecutive transversal cross sectional views of the needle tip 1900 in a case of a Hard-C tip needle with a back ground geometry. In one embodiment, the length of the needle is 1.343", the inside diameter 1906 is between 0.0138 inch and 0.0154 inch and the outside diameter 1908 is between 0.0280 and 0.0285. The tip 1900 is shown with consecutive transversal cross sectional views AA, BB, CC, DD, EE, FF, GG, MM displayed in Figures 19A, 19B, 19C, 19D, 19E, 19F, 19G and 19M. Figure 19A shows the transversal cut AA having the shape of a disc corresponding to the tube/cylindrical form of the needle. Further along approaching the tip of the needle, Figure 19D shows the cross-section DD with the back grinds 1910 at an angle of 120° in relation to the base line 1912.

Other embodiments with a back grind with an angle of  $130^\circ$  are also within the scope of the present invention.

[0070] Figure 20 shows the consecutive transversal cross sectional  
5 views of the needle tip 2000 in a case of a Hard-C tip needle with a front  
ground geometry. In one embodiment, the length of the needle is 1.343", the  
inside diameter 2002 is between 0.0155 inch and 0.0170 inch and the outside  
diameter 2004 is between 0.0280 and 0.0285. The tip 2000 is shown with  
consecutive transversal cross sectional views AA, BB, CC, DD, EE, FF, MM  
10 displayed in Figures 20A, 20B, 20C, 20D, 20E, 20F, 20M. Figure 20A shows  
the transversal cut AA having the shape of a disc corresponding to the  
tube/cylindrical form of the needle, notice the cylindrical wall of the needle is  
thinner than in the previous embodiment. Further along approaching the tip of  
the needle, Figure 20D shows cross-section DD with the front grinds 2010 at  
15 an angle of between about  $25^\circ$  and  $35^\circ$  and preferably  $30^\circ$  in relation to the  
base line 2015.

[0071] Tests show that the hard C-tip needle configuration can  
substantially eliminate coring when used in conjunction with softer springs  
20 that allow the tip of the needle to "flow" more easily inside the seal material.  
Combination of geometry elements for the C-tip such as back-ground  
geometry and hard C-tip configuration in conjunction with the use of softer  
springs, having a K spring constant between 1.5 lb/in and 6.5 lb/in, more  
preferably between 3 lb/in and 5 lb/in, provides enhanced performance of the  
25 needle in reducing coring.

[0072] Figure 21 shows a longitudinal sectional view of the needle tip  
2100 coated with a conformal coating 2200 (shown in Figure 22). A  
conformal coating is coating that conforms to the shape of the substrate while  
30 allowing blunting of sharp edges. In one embodiment, conformal coating

2200 consists of a Parylene coating (shown in Figure 22). Parylene is a registered trademark of polyparaxylylene coating, manufactured by Specialty Coating Systems, Inc. of Indianapolis, Indiana. The application of Parylene in coating an injection device and needle is described in US Pat. 5,354,286 which is incorporated herein by reference. Figure 22 shows a close up view of needle heel 2102. Membrane coring occurs when the needle heel 2102 cuts the outer surface of the seal. A rounded, or blunted, edge on the heel alleviates coring. Standard needles receive an abrasive blast during manufacturing however this blast is not sufficient since standard needles still create cores. Tests show that Parylene coating 2200 conforms well to the substrate geometry, including edges, for example edge 2202, as shown in Figure 22.

[0073] Parylene coating is applied at various thicknesses ranging from 0.0001 to 0.001 inch. Data collected in the study of effect of Parylene coating thickness on coring is summarized in graph shown in Figure 23. The graph particularly shows that Parylene coating overall decreases the likelihood of coring as well as decreases the size of the core. However, as seen on the graph, increasing the coating thickness beyond around 0.0005" does not help in decreasing coring but acts in the opposite manner by increasing coring. Indeed, the graph in Figure 23 clearly shows a curve minimum indicating that the optimum thickness of the coat accomplishing the desired results is a Parylene coating thickness around 0.0005". In addition, tests have shown that the use of a spring having a spring constant between 1.5 lb/inch and 6.5 lb/inch in conjunction with the use of a needle coated with Parylene is particularly beneficial in reducing coring.

[0074] Figure 24 shows a longitudinal sectional view of a cartridge assembly 2400 used in an automatic injector according to another embodiment of the present invention. Automatic injector uses an alternative mechanism for

reducing the rate of acceleration of the needle thus slowing down the speed of the needle in comparison with prior art devices. The acceleration rate is reduced so that the speed of the needle is less than 680 inches/s when the needle pierces the seal. The reduction in acceleration rate is intended  
5 specifically to reduce the speed to a level at which coring will not occur. Preferably, the speed at which the seal is pierced is also greater than 150 inches/s so that the injection operation is not delayed more than what is desirable. Indeed, damping disk 2402 attached to needle 2404 is used to  
10 reduce the rate of acceleration of needle 2404 by the friction generated when disk 2402 flows inside liquid medicament 2406. In other words, the flow resistance generated by the viscosity of the fluid liquid medicament against the movement of damping disk 2402 acts to reduce the rate of acceleration of  
15 needle 2404. Therefore, similarly to the previous embodiments, the damping disk plays the role of friction for slowing the tip of the needle, hence ultimately to substantially eliminating coring.

[0075] The Table below shows examples of geometries for various  
embodiments of the tip of the needle. The primary angle is selected between  
13 to 18 degrees. The bend angle, that is the angle between a tangent to a  
20 curvature of the outer surface of the end tip of the needle and a longitudinal axis of the needle, is selected to be between 51° and 100°, preferably between 85° and 95°, most preferably 90° (Figure 14 shows a bend angle of  
approximately 63° and Figure 17 shows a bend angle of approximately 90°).  
The tip offset in relation to the wall of the needle is between .024 and .026  
25 inches. The opening length is selected between .033 and .055 inches. The inside diameter is selected between .011 and .016 inches. The ratio length of opening to outside diameter of passage is between 1.7 to 2.2.

|                             | Primary<br>Angle<br>(deg)                                                         | Bend Angle<br>(tangent @ tip)<br>(deg)                                            | Opening<br>Length<br>(in)                                                         | Inside<br>Diameter<br>(in)                                                         | Ratio,<br>L/OD                                                                      | Tip Offset<br>(in) |
|-----------------------------|-----------------------------------------------------------------------------------|-----------------------------------------------------------------------------------|-----------------------------------------------------------------------------------|------------------------------------------------------------------------------------|-------------------------------------------------------------------------------------|--------------------|
|                             |  |  |  |  |  |                    |
| 10010 (Hard-C)              | 14                                                                                | 63, 81                                                                            | .081                                                                              | .016                                                                               | 2.2                                                                                 | .026               |
| 10014 (HC, Heavy Wall)      | 13                                                                                | 51, 81                                                                            | .049                                                                              | .015                                                                               | 1.7                                                                                 | .024               |
| 10017 (HC, HW, Back Ground) | 16.5                                                                              | 90, 90                                                                            | .083                                                                              | .015                                                                               | 1.9                                                                                 | .024               |
| 10018 (HC, HW, BG, B-tip)   | 13                                                                                | 80                                                                                | .053                                                                              | .011                                                                               | 1.9                                                                                 | .024               |

- [0076] While the invention has been described in connection with particular embodiments, it is to be understood that the invention is not limited to the disclosed embodiments, but on the contrary it is intended to cover
- 5 various modifications and equivalent arrangements included within the spirit and scope of the invention as defined by the claims, which follow.

THE CLAIMS DEFINING THE INVENTION ARE AS FOLLOWS:

1. An automatic injector comprising:
  - a housing having a rearward end and a forward end;
  - 5 a seal structure disposed toward the forward end of said housing;
  - a cartridge contained within said housing;
  - a charge of medicament contained in said cartridge;
  - a plunger normally disposed in a generally rearward end of said cartridge and
  - movable through said cartridge toward a generally forward end thereof in response to
  - 10 an actuating procedure, said movable plunger rearwardly confining said medicament
  - within said cartridge;
  - a needle normally disposed within said housing, said needle being projectable
  - from the forward end of said housing through said seal structure, said needle being
  - communicable with said medicament so that movement of said plunger through said
  - 15 cartridge forces said medicament through said needle and into the flesh of an
  - individual in response to said predetermined actuating procedure; and
  - a releasable energy source releasable in response to said predetermined
  - actuating procedure to project said needle from the forward end of the housing and
  - slidingly drive said plunger through said cartridge in sealed relation to expel said
  - 20 medicament through said needle and into the flesh of an individual, said cartridge
  - having an increased friction region for engaging said plunger so as to temporarily slow
  - the motion of said plunger as said plunger travels through the cartridge when the
  - forward end of the needle travels through said seal.
- 25 2. The automatic injector as claimed in claim 1, wherein said seal structure seals a
- forward end of said cartridge.
3. The automatic injector as claimed in claim 1 or claim 2, wherein said friction
- area comprises a narrowed diameter portion in a wall of said cartridge.
- 30 4. The automatic injector as claimed in claim 1 or claim 2, wherein said friction
- area is a corrugated portion in a wall of said cartridge.

5. The automatic injector as claimed in any one of claims 1 to 4, wherein a tip of said needle is coated with polyparaxylylene.
- 5 6. The automatic injector as claimed in claim 5, wherein said polyparaxylylene coating has a thickness between about 0.0001 to 0.001 inches.
7. The automatic injector as claimed in any one of claims 1 to 6, wherein said needle is normally stored within said cartridge, in contact with said medicament.
- 10 8. The automatic injector as claimed in any one of claims 1 to 7, wherein said needle comprising:  
a hollow rigid tubing having a cylindrical wall, the cylindrical wall having an inner surface and outer surface;  
15 a lumen opening having a front pointed portion comprising a lancet shaped tip having a facet grinding at an angle;  
said tip is bent in a curve directed toward a longitudinal axis of said cylindrical wall in manner as to constitute a shield to said lumen opening.
- 20 9. The automatic injector as claimed in claim 8, wherein said tip comprises primary and secondary facets, said secondary facets ground at an angle at the inside surface of the needle.
10. The automatic injector as claimed in claim 8, wherein said tip comprises primary  
25 and secondary facets, said secondary facets ground at an angle at the outside surface of the needle.
11. The automatic injector as claimed in any one of claims 1 to 10, wherein said plunger comprises a material selected from the group of plastics and rubbers.
- 30 12. The automatic injector as claimed in any one of claims 3 to 11, wherein said plunger comprises ribs arranged to reduce the rate of acceleration of said needle when in contact with said friction region.

13. The automatic injector as claimed in claim 11 or claim 12, wherein said plunger  
comprises a plurality of materials having different ductilities, said materials are  
5 selected to interact differently with said friction area to reduce the rate of acceleration  
of said needle.
14. The automatic injector as claimed in any one of claims 1 to 13, wherein said  
releasable energy source comprises a normally compressed spring which is released in  
10 response to said predetermined actuating procedure.
15. The automatic injector as claimed in claim 14, wherein said spring having a  
spring constant between 1.5 lb/in and 6.5 lb/in.
16. The automatic injector as claimed in any one of claims 1 to 15, wherein said seal  
structure comprises a material selected from the group of plastics and rubber.
17. An automatic injector comprising:  
a housing having a rearward end and a forward end;  
20 a seal structure disposed toward the forward end of said housing;  
a cartridge contained within said housing;  
a charge of medicament contained in said cartridge;  
a plunger normally disposed in a generally rearward end of said cartridge and  
movable through said cartridge toward a generally forward end thereof in response to  
25 an actuating procedure, said movable plunger rearwardly confining said medicament  
within said cartridge;  
a needle normally disposed within said housing, said needle being projectable  
from the forward end of said housing through said seal structure, said needle being  
communicable with said medicament so that movement of said plunger through said  
30 cartridge forces said medicament through said needle and into the flesh of an  
individual in response to said predetermined actuating procedure; said needle having a  
longitudinal axis and comprising:  
a hollow rigid tubing having a cylindrical wall defining a longitudinal passage  
therethrough, wherein said longitudinal passage extends parallel to said longitudinal

- axis substantially along the entire length of said passage, said cylindrical wall including opposing first and second wall portions, said first wall portion having a forward tip portion terminating in a forward end tip, said second wall portion terminating at a position rearwardly spaced from said end tip, said forward tip portion
- 5 being bent in a single direction in a manner to shield the entire cross-section of said longitudinal passage, said forward tip portion bent at an angle approximately between 51 degrees and 100 degrees; said angle defined as the angle between a tangent to a curvature of an outer surface at said forward end tip and the longitudinal axis of said needle;
- 10 a releasable energy source releasable in response to said predetermined actuating procedure to project said needle from the forward end of the housing and slidably drive said plunger through said cartridge in sealed relation to expel said medicament through said needle and into the flesh of an individual.
- 15 18. The automatic injector as claimed in claim 17, wherein said seal structure seals a forward end of said cartridge.
19. The automatic injector as claimed in claim 17 or claim 18, wherein the tip of said needle is coated with polyparaxylylene.
- 20 20 The automatic injector as claimed in claim 19, wherein said polyparaxylylene coating has a thickness between about 0.0001 to 0.001.
21. The automatic injector as claimed in any one of claims 17 to 20, wherein said
- 25 forward tip portion is bent at an angle approximately between 85 degrees and 95 degrees; said angle defined as the angle between a tangent to a curvature of an outer surface at said end tip and said longitudinal axis of said needle.
22. The automatic injector as claimed in claim 21, wherein said seal structure seals a
- 30 forward end of said cartridge.
23. The automatic injector as claimed in claim 21 or claim 22, wherein a line extends along an inner surface of said second wall, wherein said forward end tip intersects said line.

24. The automatic injector as claimed in any one of claims 17 to 23, wherein said second wall portion terminating at a position rearwardly spaced from said end tip, said forward tip portion being bent in a manner to shield the entire cross-section of said longitudinal passage; said needle comprises an enlarged rearward portion constructed and arranged for engagement with said plunger.
25. The automatic injector as claimed in any one of claims 21 to 24, wherein said needle comprises an enlarged rearward portion constructed and arranged for engagement with said plunger.
26. The automatic injector as claimed in any one of claims 17 to 25, wherein an opening of the needle has a heel at the termination position of the second wall portion, the heel having a rounded or blunted edge.
27. The automatic injector as claimed in claim 1, wherein said releasable energy source comprises a spring having a spring constant between approximately 1.5 lb/inch and 6.5 lb/inch.
28. A method for injecting a medicament with an automatic injector, which injector comprises a housing, a seal structure disposed toward a forward end of said housing, a cartridge contained within said housing, a charge of medicament contained in said cartridge, a plunger movable through said cartridge toward a generally forward end thereof in response to an actuating procedure, said movable plunger rearwardly confining said medicament within said cartridge, a needle normally disposed within said housing, said needle being projectable from the forward end of said housing through said seal structure, said needle being communicable with said medicament so that movement of said plunger through said cartridge forces said medicament through said needle and into the flesh of an individual in response to said predetermined actuating procedure, a releasable energy source releasable in response to said predetermined actuating procedure to project said needle from the forward end of the housing and slidably drive said plunger through said cartridge in sealed relation to expel said medicament through said needle and into the flesh of an individual;  
said method comprising:

releasing said energy source;  
accelerating said needle forwardly within said housing;  
reducing the rate of acceleration of said needle prior to said needle  
penetrating said seal; and  
5 expelling said medicament through said needle.

29. The method for injecting a medicament with an automatic injector as claimed in  
claim 28, wherein said penetrating said seal is performed at a speed between 250  
inches/s and 680 inches/s.

10 30. The method for injecting a medicament with an automatic injector as claimed in  
claim 28 or claim 29, further comprising:  
speeding up said needle after said needle has fully penetrated said seal.

15 31. A method for injecting a medicament with an automatic injector, which injector  
comprises a housing, a seal structure disposed toward a forward end of said housing, a  
cartridge contained within said housing, a charge of medicament contained in said  
cartridge, a plunger movable through said cartridge toward a generally forward end  
thereof in response to an actuating procedure, said movable plunger rearwardly  
20 confining said medicament within said cartridge, a needle normally disposed within  
said housing, said needle being projectable from the forward end of said housing  
through said seal structure, said needle being communicable with said medicament so  
that movement of said plunger through said cartridge forces said medicament through  
said needle and into the flesh of an individual in response to said predetermined  
25 actuating procedure, a releasable energy source releasable in response to said  
predetermined actuating procedure to project said needle from the forward end of the  
housing and slidably drive said plunger through said cartridge in sealed relation to  
expel said medicament through said needle and into the flesh of an individual;

said method comprising:  
30 releasing said energy source;  
moving said needle forwardly within said housing at a speed of less  
than 680 inches/s as said needle penetrates said seal; and  
expelling said medicament through said needle.

32. A method for injecting a medicament with an automatic injector as claimed in claim 31, wherein said method comprises moving said needle forwardly within said housing at a speed of more than 150 inches/s as said needle penetrates said seal.
- 5 33. The automatic injector as claimed in claim 1 or claim 17, substantially as hereinbefore described with reference to any of the Figures.
- 10 34. The method for injecting a medicament with an automatic injector as claimed in claim 28 or claim 31, substantially as hereinbefore described with reference to any of the Figures.

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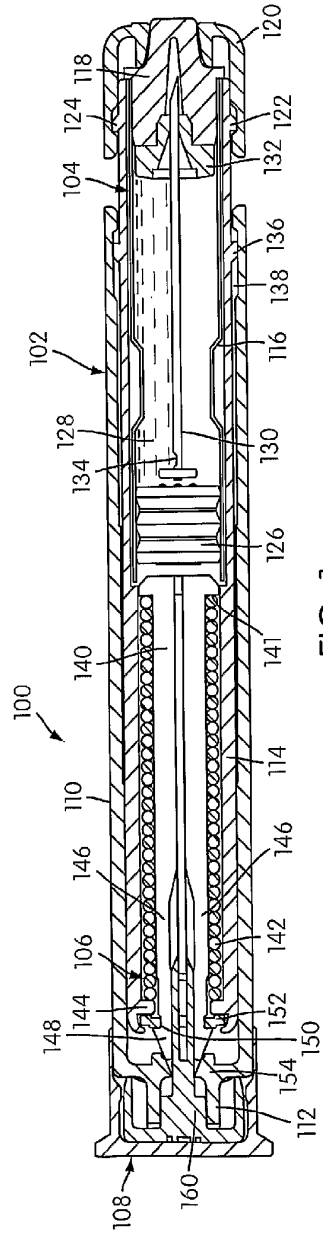
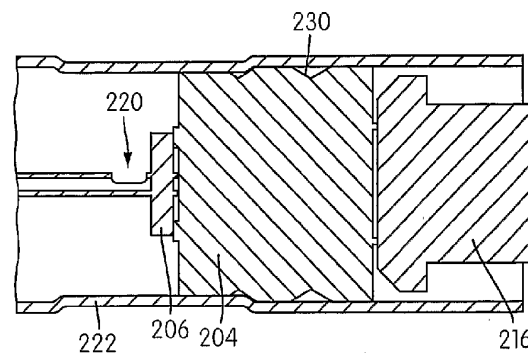
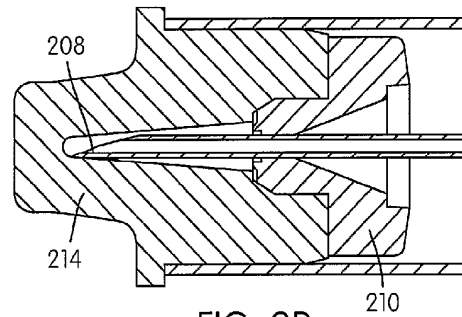
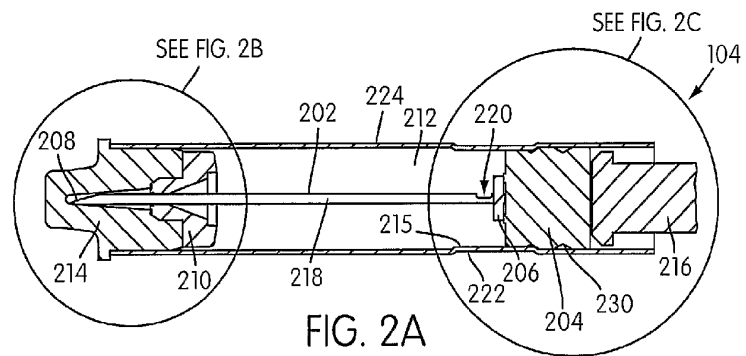


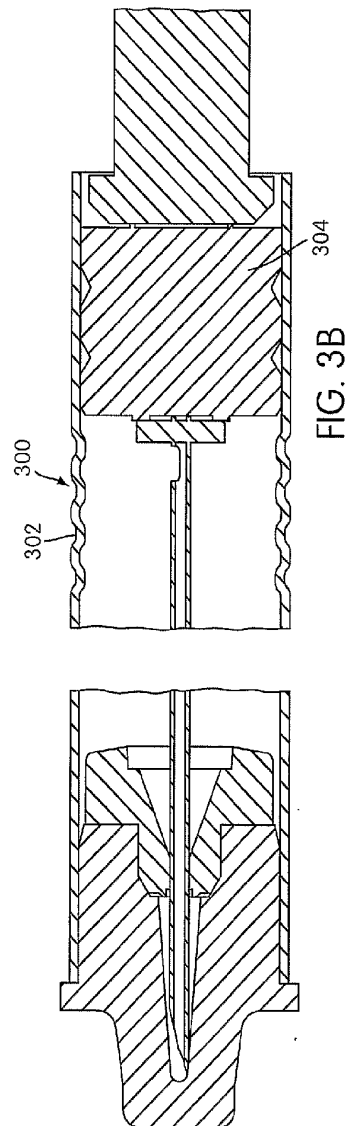
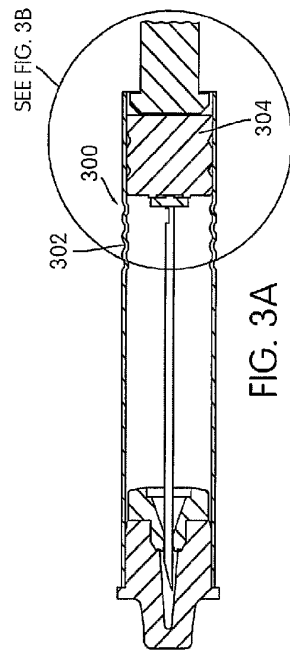
FIG. 1

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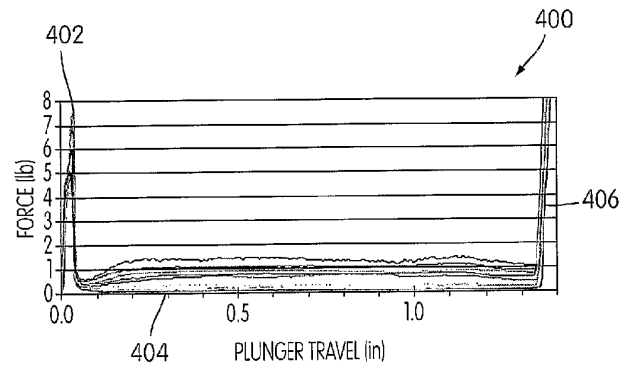


FIG. 4

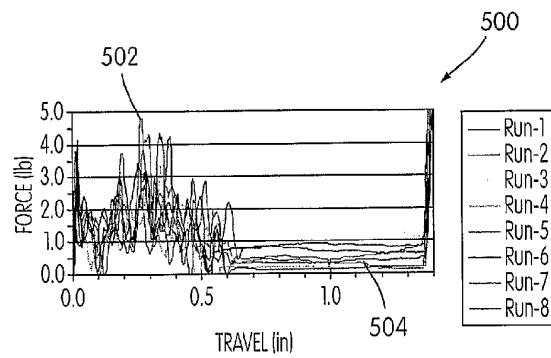


FIG. 5

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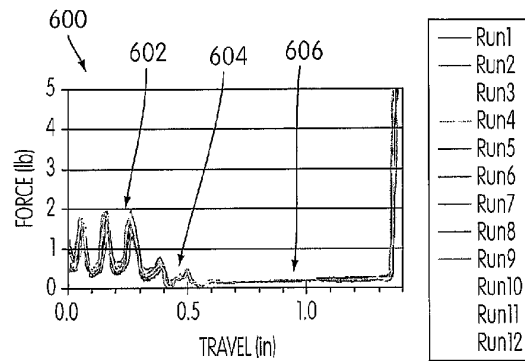


FIG. 6

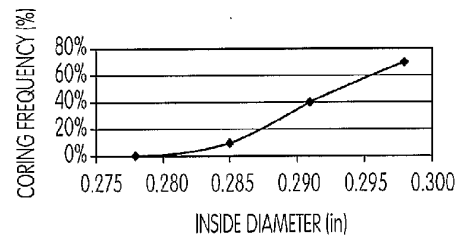


FIG. 7

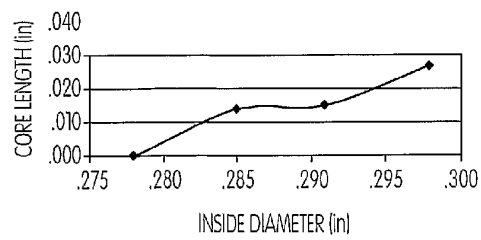


FIG. 8

SUBSTITUTE SHEET (RULE 26)

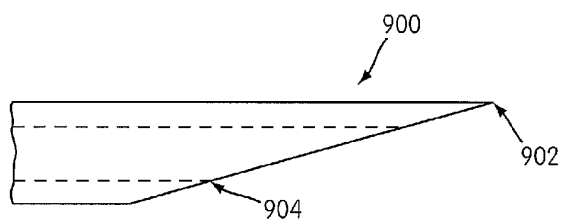


FIG. 9

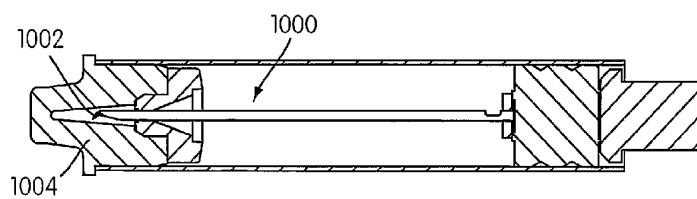


FIG. 10

SUBSTITUTE SHEET (RULE 26)

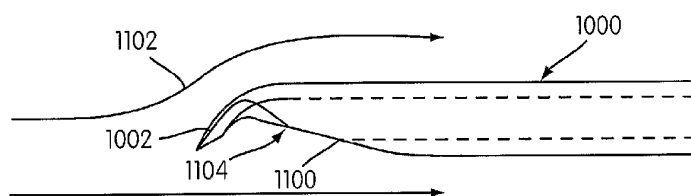


FIG. 11A

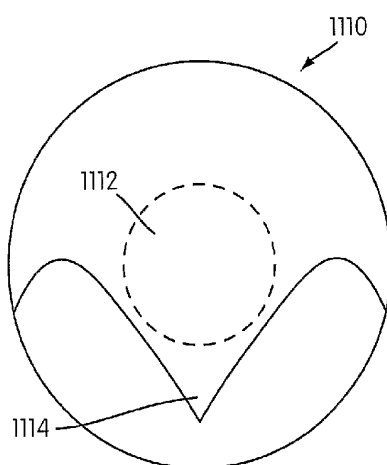


FIG. 11B

SUBSTITUTE SHEET (RULE 26)

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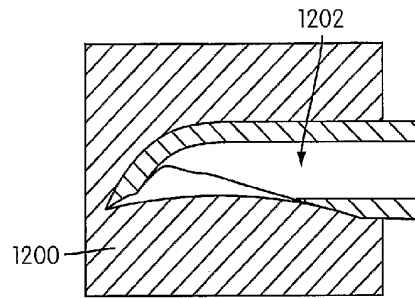


FIG. 12

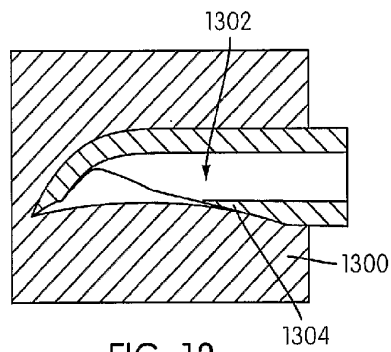


FIG. 13

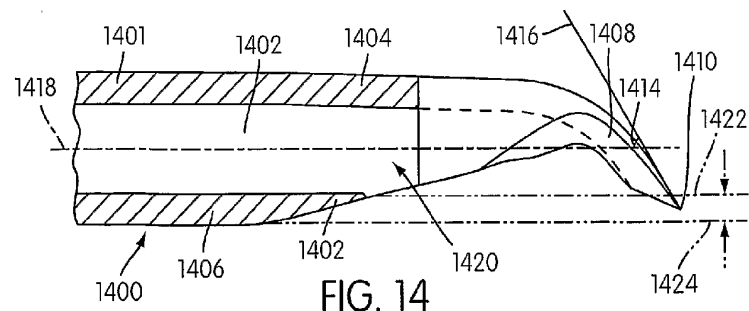


FIG. 14

SUBSTITUTE SHEET (RULE 26)

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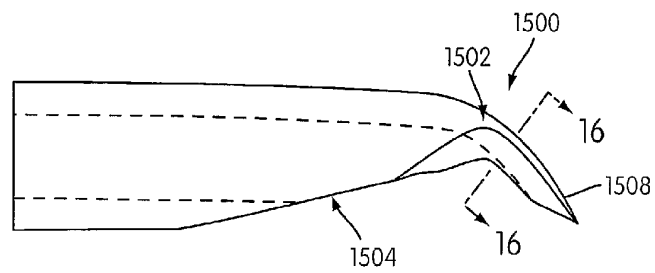


FIG. 15

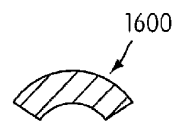


FIG. 16

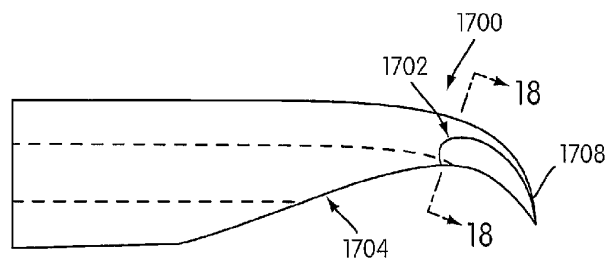


FIG. 17

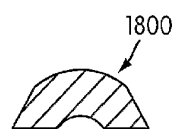


FIG. 18

SUBSTITUTE SHEET (RULE 26)

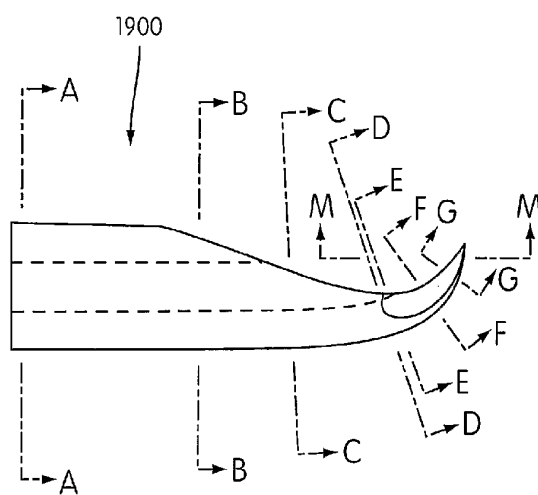


FIG. 19

SUBSTITUTE SHEET (RULE 26)

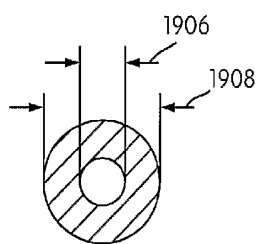


FIG. 19A

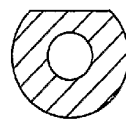


FIG. 19B



FIG. 19C

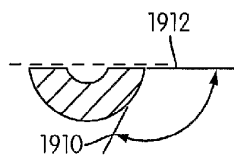


FIG. 19D



FIG. 19E



FIG. 19F



FIG. 19G



FIG. 19M

SUBSTITUTE SHEET (RULE 26)

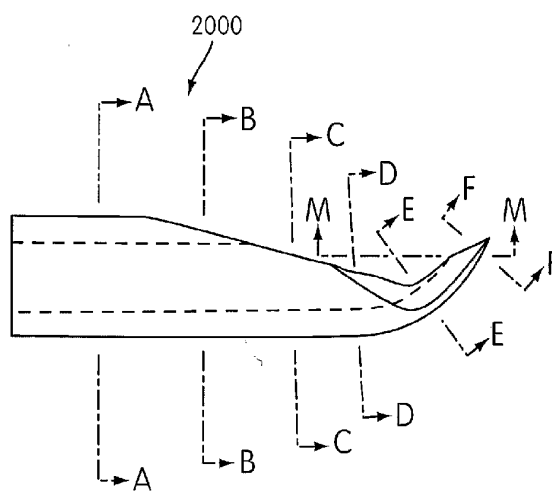


FIG. 20

SUBSTITUTE SHEET (RULE 26)

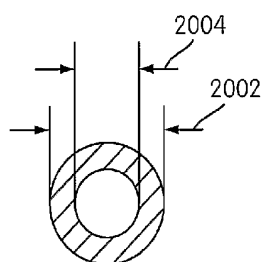


FIG. 20A

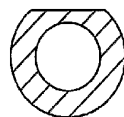


FIG. 20B



FIG. 20C

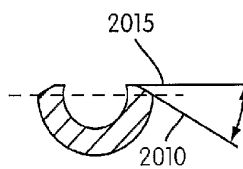


FIG. 20D



FIG. 20E



FIG. 20F



FIG. 20M

SUBSTITUTE SHEET (RULE 26)

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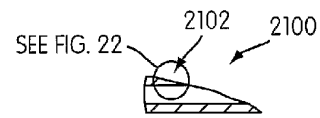


FIG. 21

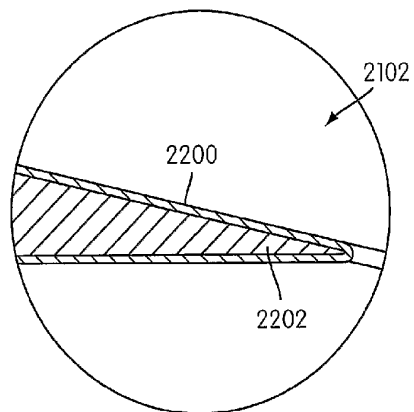


FIG. 22

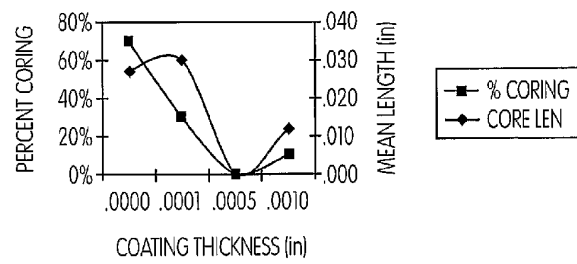


FIG. 23

SUBSTITUTE SHEET (RULE 26)

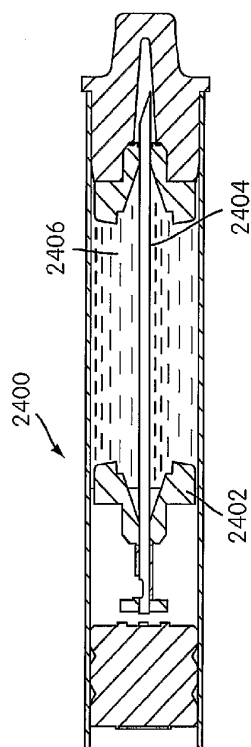


FIG. 24

SUBSTITUTE SHEET (RULE 26)