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(54) **PROSTHETIC HEART VALVE SYSTEMS**

Publication Classification

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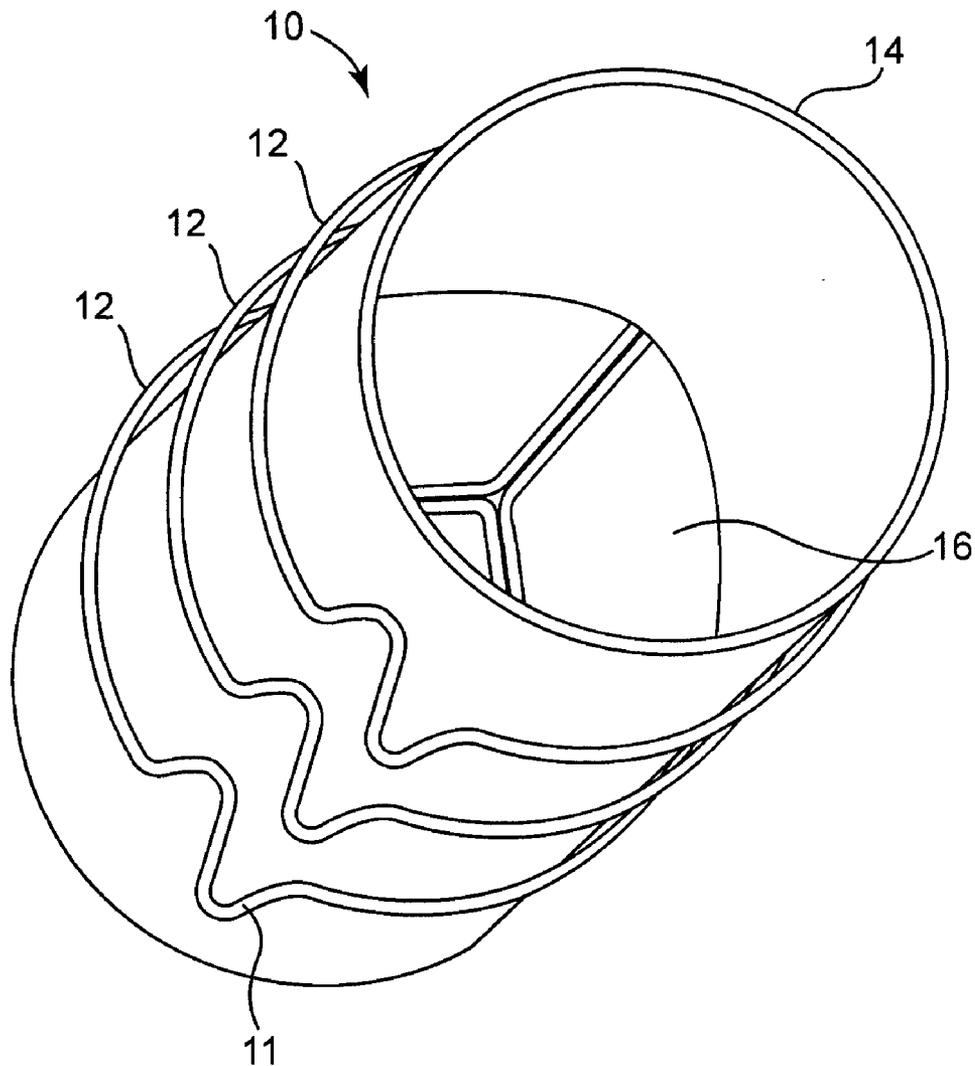
(57) **ABSTRACT**

A heart valve that can be expanded following its implantation in a patient, such as to accommodate the growth of a patient and the corresponding growth of the area where the valve is implanted, and to minimize paravalvular leakage. In one aspect, the invention may maximize the orifice size of the surgical valve. The invention includes expandable implantable conduits and expandable bioprosthetic stented valves. In one aspect of the invention, the valve may be adapted to accommodate growth of a patient to address limitation on bioprosthetic valve lifespans.

(21) Appl. No.: **12/380,483**
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Related U.S. Application Data

(60) Provisional application No. 61/032,185, filed on Feb. 28, 2008.



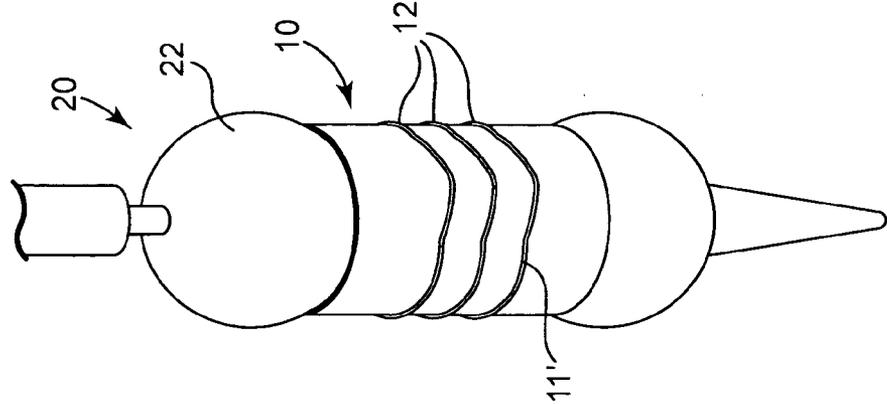


Fig. 2

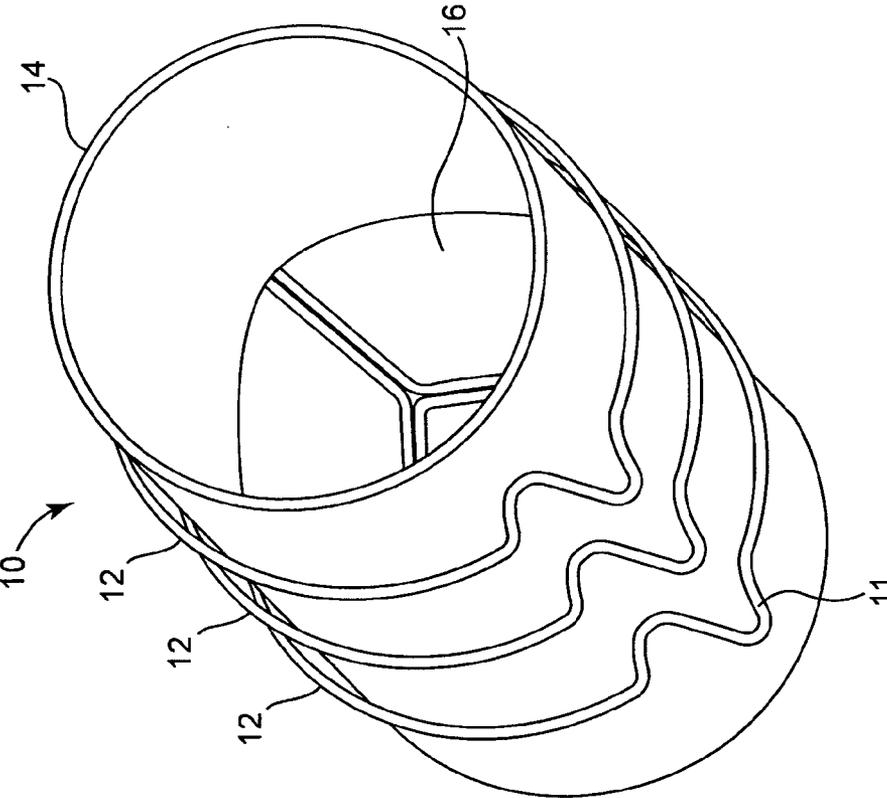


Fig. 1

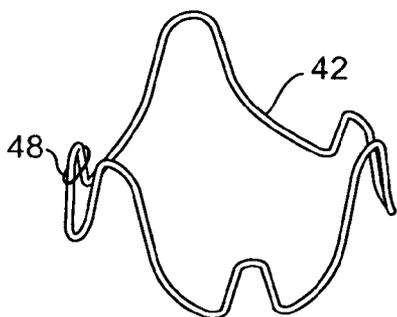


Fig. 3

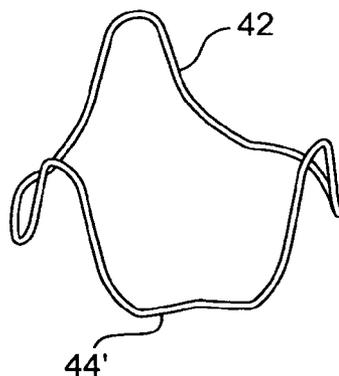


Fig. 6

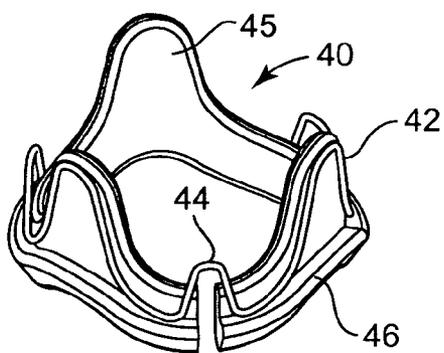


Fig. 4

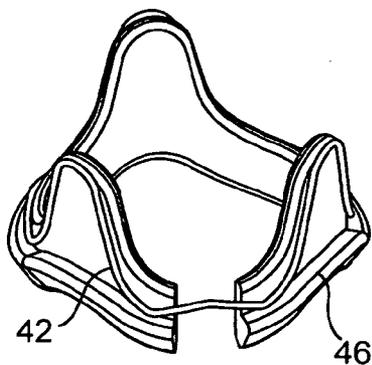


Fig. 5

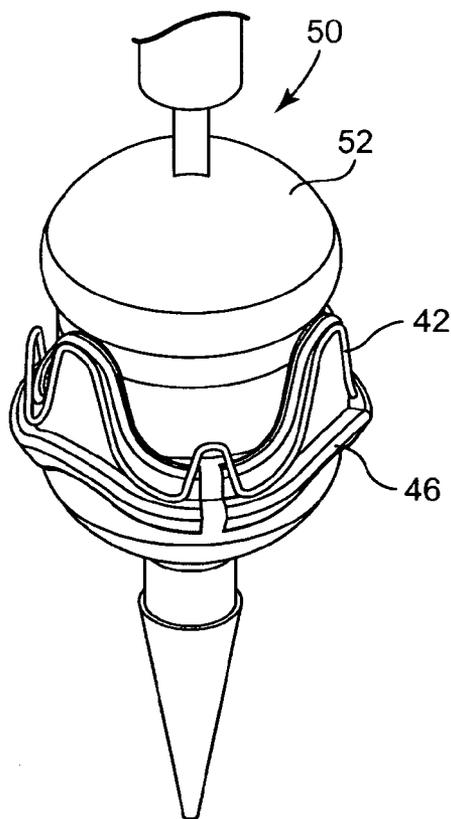


Fig. 7

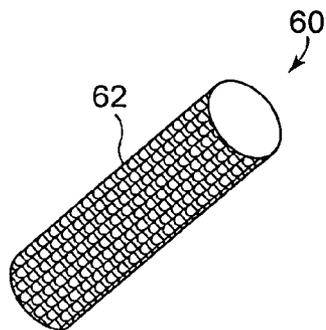


Fig. 8

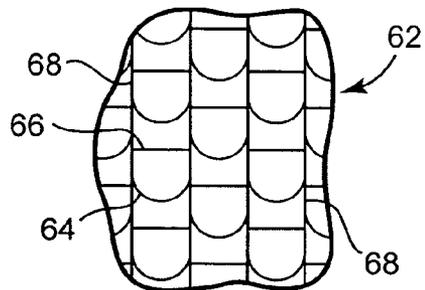


Fig. 9

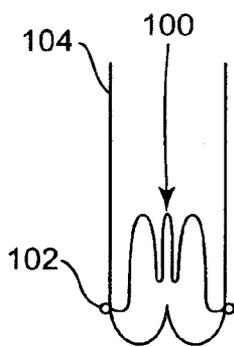


Fig. 10

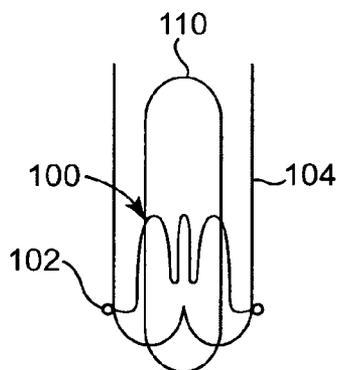


Fig. 11

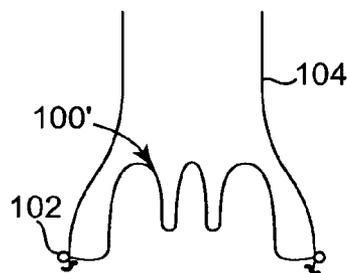


Fig. 12

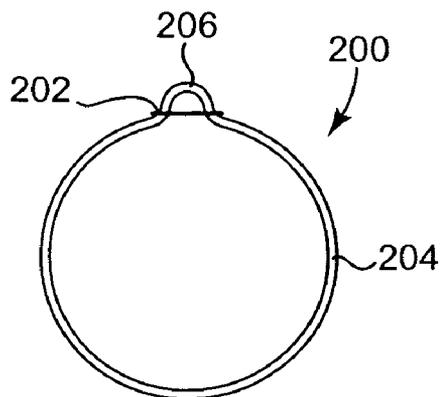


Fig. 13

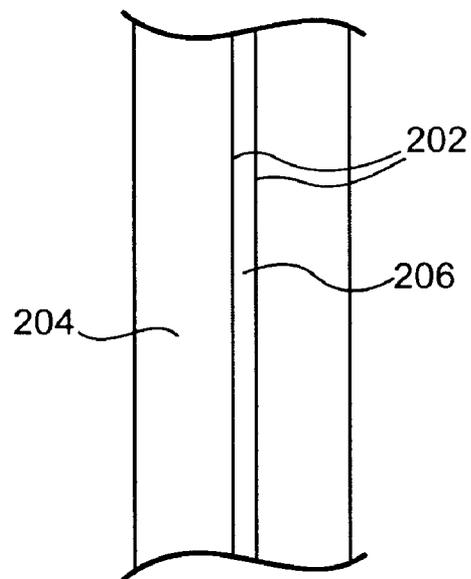


Fig. 14

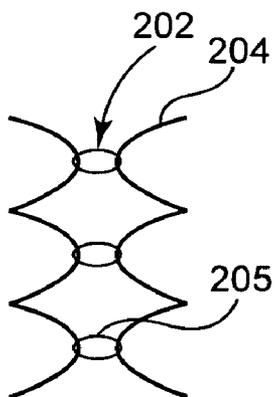


Fig. 15

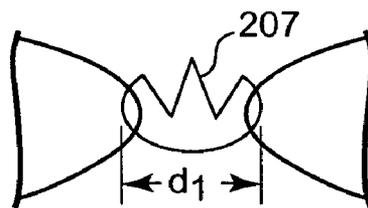


Fig. 16

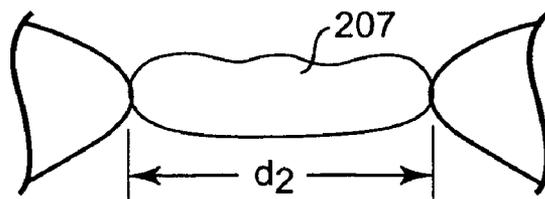


Fig. 17

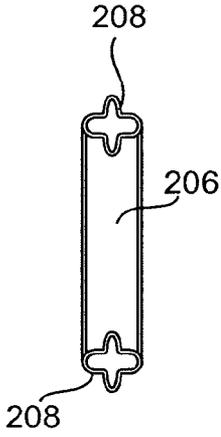


Fig. 18

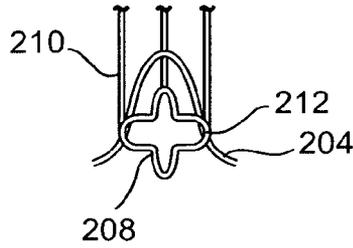


Fig. 19

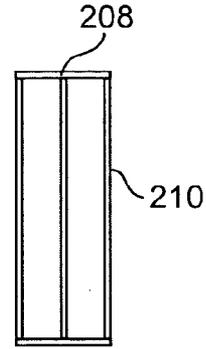


Fig. 20

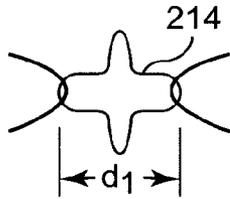


Fig. 21

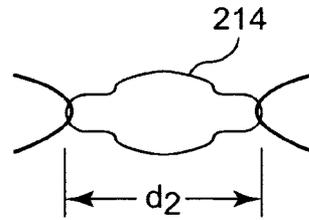


Fig. 22

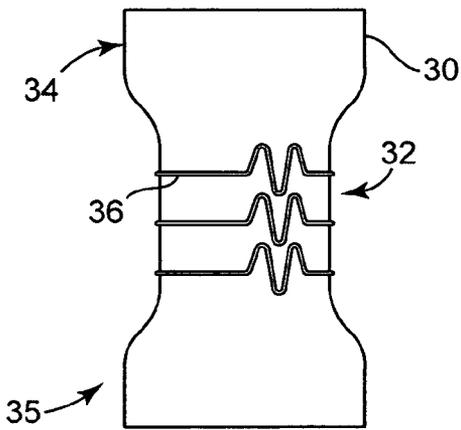


Fig. 23

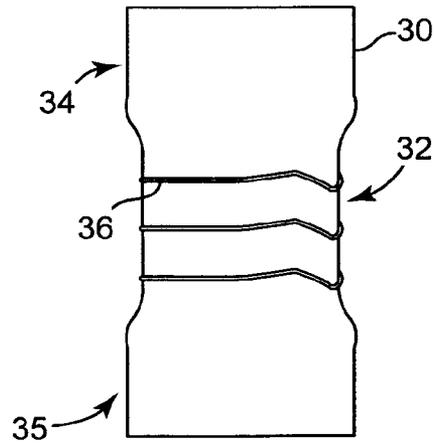


Fig. 24

PROSTHETIC HEART VALVE SYSTEMS

CROSS-REFERENCE TO RELATED APPLICATION

[0001] The present application claims priority to U.S. Provisional Application No. 61/032,185, filed Feb. 28, 2008, and titled "Prosthetic Heart Valve Systems," the entire contents of which is incorporated herein by reference in its entirety.

TECHNICAL FIELD

[0002] The present invention relates to prosthetic heart valves. More particularly, it relates to transcatheter implants, methods, and delivery systems.

BACKGROUND

[0003] Heart valve replacement surgery involves the replacement of the native valves of the heart with a prosthetic valve. Prosthetic valves include mechanical valves involving only metals and polymers, and tissue valves that include non-synthetic, biocompatible materials such as pericardium, or bovine, equine or porcine tissue. Some patients have a relatively small aortic root due to their particular anatomy or excessive calcification. Some patients (e.g., young children) are likely to outgrow a prosthetic valve or outlive the useful life of a prosthetic valve.

[0004] U.S. Pat. No. 5,383,926 (Lock et al.) discloses a re-expandable endoprosthesis. The endoprosthesis is said to be re-expandable to accommodate vessel change.

[0005] U.S. Patent Application Publication Nos. 2003/0199971 A1 (Tower et al.) and 2003/0199963 A1 (Tower et al.) describe a valved segment of bovine jugular vein mounted within an expandable stent, for use as a replacement heart valve. Replacement pulmonary valves may be implanted to replace native pulmonary valves or prosthetic pulmonary valves located in valved conduits as described, for example, in "Percutaneous Insertion of the Pulmonary Valve", Bonhoeffer, et al., *Journal of the American College of Cardiology* 2002; 39: 1664-1669.

[0006] Degenerated and stenotic valves in conduits or in valved stents potentially allow for a second valved stent implantation without the need for surgery, as described, for example, in "Transcatheter Replacement of a Bovine Valve in Pulmonary Position", Bonhoeffer, et al., *Circulation* 2000; 102: 813-816. It has been proposed that sequential percutaneous pulmonary valve implantation is feasible and theoretically could delay the need for invasive surgery indefinitely, thus overcoming concerns regarding conduit longevity and risks associated with reoperation, as described, for example, in "The potential impact of percutaneous pulmonary valve stent implantation on right ventricular outflow tract re-intervention", Coates, et al., *European Journal of Cardio-thoracic Surgery* 27 (2005) 536-543.

[0007] U.S. Patent Application Publication No. 2003/0199971 A1 (Tower et al.) discloses a stented valve with an ability to be reconfigured after implantation. This is identified as a feature useful in cases where a valve has been implanted in a growing patient (e.g., a child). Rather than replacing a valve periodically during the growth period, the supporting stent may be reconfigured to accommodate growth using a percutaneously introduced balloon catheter for re-engaging the stent to reconfigure the stent so that it will conform to the changes in the implantation site produced by the growth of the patient. In an article by Bonhoeffer, et al. entitled "Percuta-

neous Insertion of the Pulmonary Valve" *J Am Coll Cardiol*, 2002; 39:1664-1669, the percutaneous delivery of a biological valve is described. The valve is sutured to an expandable stent within a previously implanted valved or non-valved conduit, or a previously implanted valve. Again, radial expansion of the secondary valve stent is used for placing an maintaining the replacement valve.

[0008] Stented valve systems involving two or more components are disclosed in U.S. Patent Application Nos. 2004/0030381 A1 (Shu et al.) and 2008/0004696 A1 (Vesely et al.); U.S. Pat. Nos. 6,530,052 (Khou et al.) and 7,011,681 (Vesely et al.) and PCT Publication Nos. WO 06/0127756 A2 (Rowe et al.), WO 07/018,1820 (Nugent et al.) and WO 07/130,537 (Lock et al.). Some of these valve systems describe the reuse of a portion of their system. Some of these valve systems require the removal of an element and its replacement by a different element. It is believed that transcatheter removal of a previously implanted stented valve component creates challenges such as damage to implant site, creation of sites for thrombus/emboli formation and release, paravalvular leakage, inability to access removable elements due to tissue ingrowth and/or complex navigation, and delivery difficulties.

SUMMARY

[0009] The present invention is directed to a heart valve that can be expanded following its implantation in a patient. In one aspect of the present invention, the expansion can accommodate the growth of a patient and the corresponding growth of the area where the valve is implanted. In another aspect, the present invention may maximize the orifice size of the surgical valve. The present invention includes expandable implantable conduits and expandable bioprosthetic stented valves. In one aspect of the invention, the valve may be adapted to accommodate growth of a patient to address limitation on bioprosthetic valve lifespans.

[0010] The heart valves of the invention may also facilitate a subsequent minimally invasive intervention for replacement of all or part of the valve system. In another aspect, the heart valves of the invention may ease the implantation process and could accommodate the use of a larger valve, which is especially useful for a patient with a small annulus (e.g., a small aortic annulus).

[0011] The heart valves of the invention have the capacity to overcome concerns regarding conduit longevity and risks associated with performing multiple surgeries in the same area of the patient. The heart valves of the present invention advantageously utilize the proven attributes of surgical valves (e.g., durability), while addressing some of the shortcomings of surgical valves. In particular, the heart valves of the invention provide the ability to expand a valve post implant, which provides a number of major advantages that have yet to be proven clinically in humans. First, surgical tissue valves are typically offered in a limited number of sizes/diameters. The post-implant transcatheter surgical valve expansion provided by the valves of the invention enables the orifice size for each surgical prosthetic valve patient to be maximized post-implant, thereby improving valve function. Second, the post-implant surgical valve transcatheter expansion provided by the valves of the invention enables the orifice for each surgical prosthetic valve pediatric patient to be adjusted post-implant, to thereby accommodate patient growth and eliminate unnecessary surgeries. Third, the post-implant transcatheter surgical valve expansion provided by the valves of the invention

increases the orifice size of the surgical prosthetic valve patient to accommodate a larger transcatheter valve after failure of the surgical valve, thereby eliminating the need for surgical replacement. Fourth, the post-implant transcatheter surgical valve expansion provided by the valves of the invention enables clinicians to implant transcatheter valves inside small bioprosthetic valves with improved hemodynamic results. Fifth, the post-implant transcatheter surgical valve expansion provided by the valves of the invention may enable implantation of bioprosthetic valves into younger patients by facilitating transcatheter valve replacement once the bioprosthetic valve fails or presents severe risk of failure.

[0012] In another aspect of the invention, surgical methods are provided. In one embodiment, the method comprises implanting a surgical valve in an efficient manner. For example, some patients have a small aortic annulus. The present invention affords implantation of a valve in an under-sized condition, after which the valve may be expanded to be larger in size or diameter (e.g., with a balloon), such as after the patient grows, minimizing the need for re-operation due to inadequate orifice size.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013] The present invention will be further explained with reference to the appended Figures, wherein like structure is referred to by like numerals throughout the several views, and wherein:

[0014] FIG. 1 is a perspective view of an expandable valved conduit in its relatively compressed state, according to one aspect of the invention;

[0015] FIG. 2 is a perspective view of the expandable valved conduit of FIG. 1 in its relatively expanded state, along with a balloon expandable member positioned within the conduit;

[0016] FIG. 3 is a perspective view of an expandable stent or member or frame for a stented valve in its relatively compressed state, according to another aspect of the invention;

[0017] FIG. 4 is a perspective view of the stent of FIG. 3 assembled to additional components of a valve assembly, with the stent in a first implantable configuration. The fabric covering is removed from the frame of the valve assembly in the area of an expansion joint for illustration purposes;

[0018] FIG. 5 is a perspective view of the assembly of FIG. 4 with the stent or member or frame expanded from the first implantable configuration to a second implantable configuration;

[0019] FIG. 6 is a perspective view of the stent or member or frame of FIG. 5;

[0020] FIG. 7 is a perspective view of a balloon expandable member positioned within a valve assembly that is configured as is generally shown in FIGS. 3 and 4;

[0021] FIG. 8 is a perspective view of an expandable component of another embodiment of the invention;

[0022] FIG. 9 is an enlarged front schematic view of a portion of the expandable component of FIG. 8;

[0023] FIG. 10 is a front schematic view of an embodiment of a heart valve of the invention that is implanted in a first, unexpanded condition;

[0024] FIG. 11 is a front schematic view of a balloon being used to expand the heart valve of FIG. 10 toward an expanded condition;

[0025] FIG. 12 is a front schematic view of the heart valve of FIG. 10 after it has been expanded;

[0026] FIG. 13 is a top view of an expandable tubular component according to another aspect of the invention;

[0027] FIG. 14 is a side view of a portion of the component of FIG. 13;

[0028] FIG. 15 is an enlarged side view of a portion of FIG. 14;

[0029] FIG. 16 is another embodiment of a side view of an expandable seam of the invention, with the seam in a relatively unexpanded condition;

[0030] FIG. 17 is a side view of the seam of FIG. 16 in a relatively expanded condition;

[0031] FIG. 18 is a partial cross-sectional view of a seam expansion member of the invention;

[0032] FIG. 19 is a bottom perspective view of a portion of the expansion member of FIG. 18;

[0033] FIG. 20 is a front view of the expansion member of FIG. 18;

[0034] FIG. 21 is a side view of another embodiment of an expansion member of the invention;

[0035] FIG. 22 is another side view of the expansion member of FIG. 21;

[0036] FIG. 23 is a front view of another embodiment of an expandable conduit of the invention in a relatively unexpanded state; and

[0037] FIG. 24 is a front view of the conduit of FIG. 23 in a relatively expanded state.

DETAILED DESCRIPTION

[0038] FIG. 1 shows an assembly 10 comprising a plurality of circumferential support structures 12 and a valved conduit 14. The valved conduit 14 may comprise any suitable implantable valve conduit such as those utilizing bovine, equine, human, or porcine tissue, or other materials, such as polymeric and/or metallic materials. The conduit 14 may comprise an outer tubular structure within which multiple leaflets 16 are positioned. For example, the component of the valved conduit may comprise the Medtronic Freestyle (or Contegra) Implantable Valved Conduit, which is commercially available from Medtronic, Inc. of Minneapolis, Minn. However, it is also possible with the various embodiments of the invention that a valve having a single leaflet or moveable component is utilized within a valve conduit or other valve structure, including tissue valves or mechanical valves.

[0039] The support structures 12 may be attached to the outside surface of the outer tubular structure of the valved conduit 14 using conventional means, such as sutures, clips, adhesives, molding, weaving, and the like. Alternatively, the support structures 12 can be attached inside or be positioned within the conduit 14, such as can be accomplished with a molded elastomer or woven fabric.

[0040] The support structures 12 described herein can comprise a series of synthetic elements, mesh wires or wire segments. They can be independent or connected to each other via a link that can be permanent or temporary. The support structures 12 may be constructed from a number of suitable biocompatible materials such as polyester, materials such as the membrane "Gore-Tex", which is commercially available from W.L. Gore & Associates, Inc. of Elkton, Md., stainless steel, titanium, cobalt chromium alloy, platinum iridium, or other natural or man-made materials. Each support structure 12 may be unitary or homologous in composition or could comprise different segments made of different materials. The portion of each support structure 12 that allows or provides for its expansion may comprise a different geometry than the

remaining portion of that support structure **12**, or it may comprise a more malleable or deflectable portion. Each support structure **12** of a particular assembly **10** may be identical or similar to at least one other support structure **12** of that same assembly **10**, or each support structure **12** of an assembly **10** may be different from the other support structures **12** of the assembly **10** in size, shape, material, and/or other characteristics. In one embodiment of an assembly **10** of the invention, all of the support structures **12** are identical in size, shape and composition. The support structures **12** will desirably be designed to provide sufficient support to hold the conduit diameter to a reasonably constant diameter, thereby enabling proper function and durability of the valve. Any number of configurations or structures can be used, such as those that can be laser cut, knitted, braided, or woven, for example. In addition, the support structures **12** will desirably be able to support the valve for changes in diameter at a minimum number of commissures and inflow regions of the valve. It is further desirable that the support structures are visible or detectable when using common medical imaging techniques, such as fluoroscopy, echocardiography, magnetic resonance imagery, and the like.

[0041] The elements of the support structures in other embodiments can alternatively be formed from a shape memory material such as nickel titanium alloy (e.g., Nitinol). With this material, the support structure is self-expandable from a contracted state to an expanded state, such as by the application of heat, energy, and the like, or by the removal of external forces (e.g., compressive forces).

[0042] The support structures **12** are adapted to be implanted in a patient in the generally cylindrical shape shown in FIG. 1, although the support structures **12** may instead have an outer shape that is oval, elliptical, irregular, or another shape that is chosen to be appropriate for the location in the patient where it will be implanted. The assembly **10** is configured so that it can be altered at any time after it is initially implanted within a patient. For example, the assembly **10** can be expanded immediately after a procedure of suturing the assembly **10** to the patient's anatomy in order to maximize the size of the orifice in which it is implanted. Alternatively, the assembly **10** could be expanded at some period of time after the initial implantation procedure, such as at the end of the useful life of the tissue of the valved conduit **14** or upon growth of the patient. In another embodiment, a first assembly **10** is implanted in a patient using an initial implantation procedure, then after some period of time (e.g., several months or years), a second procedure may be performed to expand the support structures **12** to the configuration of FIG. 2. This expanded configuration can then receive a second or replacement assembly **10** within its interior structure, if desired.

[0043] In one embodiment, the support structures **12** should be sufficiently strong to withstand the foreseeable stresses that may be encountered at the implantation site after the assembly **10** is implanted without any undesirable degradation that would result in conduit rupture and/or valve failure. However, the support structure **12** may be designed so that it will deflect in vivo from the configuration shown in FIG. 1 to that shown in FIG. 2 under the influence of a force that can be provided by an expandable assembly **20**, for example. Expandable assembly **20** comprises an expandable balloon member **22**. The balloon member **22** can be a high pressure, non-compliant balloon, such as a Numed Z-Med or Mullins valvuloplasty balloon, for example, although a wide

variety of other types and manufacturers of balloons can be used. The balloon member **22** can be sized to produce a desired expansion of the support structure **12**. The balloon member could be provided with various sizes and/or shapes to produce conduits of various sizes and/or shapes. The structure of the balloon member can be capable of expanding by various degrees and/or amounts within a prescribed range in order to provide for proper valve function. In one embodiment of the invention, the support structures **12** expand by deflection of the portions **11** from the configuration in FIG. 1, to the configuration **11'** in FIG. 2. In this case, the entire conduit is uniformly expanded via expansion of the assembly **20**.

[0044] In another embodiment, the expandable assembly **20** includes an expansion member that is not a balloon, but is a system having other components that can exert radial forces on the support structures so that they can be expanded to a larger diameter. For example, the expandable assembly may include a self-expanding stent that is capable of being compressed, positioned within the interior area of the support structures, and then released within the support structures. The self-expanding stent is designed so that it can thereby exert sufficient outward radial force when positioned within the support structures to diametrically deform and/or expand the support structures, in accordance with the various embodiments of the invention.

[0045] An alternative embodiment of a conduit **30** is illustrated in FIGS. 23 and 24. Conduit **30** includes a central area **32** that is at least slightly smaller in diameter than the end portions **34**, **35** when the conduit is initially implanted. This central area **32** is the portion of conduit **30** in which valve leaflets can be positioned. Expandable support structures **36** are longitudinally spaced from each other in the central area **32**, where the structures **36** are in their relatively expanded condition in FIG. 23 and in their relatively expanded condition in FIG. 24. An expansion mechanism (e.g., balloon) can be used to expand the central area **32** to a diameter that is closer to that of the end portions **34**, **35**, thereby making the conduit **30** more cylindrical in shape.

[0046] FIGS. 3 through 7 disclose an expandable support structure component **42** of the invention, as positioned relative to a stent or valve structure **40**. Valve structure **40** includes a sewing ring **46** attached to three stent posts or commissural members **45**. It is noted that this structure would be provided for a tricuspid valve, but that only two of such commissural members would be provided for a bicuspid valve, in another embodiment. All or a portion of the valve structure **40**, including the sewing ring **46** and commissural members **45**, can be covered by a flexible covering, which may be a tissue, polymer, fabric, metal, or cloth material to which leaflets (not shown) of the heart valve can be sewn. Further, as is known in the art, the internal structure of each of the commissural members **45** can be formed of a stiff but resiliently bendable material. This construction allows the commissural members **45** to be deflected by the application of an external or internal radial force.

[0047] The valve structure **40** is generally tubular in shape, defining an internal area that extends from an inflow end to an outflow end. Alternatively, the shape of the valve structure can be oval, elliptical, irregular, or any other desired shape. The internal area is essentially composed of the valve structure **40**, and the valve structure **40** selectively allows for fluid flow into or out of the lumen of the natural heart valve in which it is implanted. Thus, the internal area is alternatively

open and closed to the lumen of the natural heart valve in which it is inserted via movement of leaflets. For ease of illustration, leaflets associated with valve structure 40 are not shown in FIGS. 4 and 5.

[0048] As referred to herein, the prosthetic heart valves (e.g., valves that utilize a valve structure 40) used in accordance with the devices and methods of the invention may include a wide variety of different configurations, such as a prosthetic heart valve having one or more tissue leaflets, a synthetic heart valve having polymeric leaflets, or a mechanical valve, and can be specifically configured for replacing any heart valve. That is, the prosthetic heart valves of the invention can generally be used for replacement of aortic, mitral, tricuspid, or pulmonic valves, for use as a venous valve, or to replace a failed bioprosthesis, such as in the area of an aortic valve or mitral valve, for example. The replacement prosthetic heart valves of the invention can be employed to functionally replace stentless bioprosthesis heart valves as well.

[0049] The support structure 42 is part of the valve structure 40 and includes portions that generally follow the shape of the stent posts 45. Arch or member 44 of the support structure 42 can be deformed or modified after the valve structure 40 has been implanted to effectively enlarge the size of the orifice of the valve structure 40. In an initial implanted configuration, the support structure 42 may comprise the shape shown in FIGS. 3-4 and 7. In a subsequent procedure (which could potentially be any period of time later, such as minutes, hours, days, months or years), the shape of the support structure 42 can be modified such that member 44 shown in FIGS. 3 and 4 assumes the shape shown as member 44' in FIGS. 5 and 6. In this way, the internal area or diameter of the support structure 42 will be larger in order to provide the maximum available orifice area based on the patient's anatomy. In addition, expansion of the support structure 42 can put the valve structure in closer contact with the vessel anatomy, thereby improving the paravalvular seal, which can thereby reduce the degree of paravalvular leakage. Expansion of the support structure can also improve the stability of the surgical valve implant, which can reduce the chances for dehiscence. It is contemplated that an intermediate deformation of the member 44 can also occur so that the internal area has a size that is between that shown in FIGS. 4 and 5. It should be noted that the shape of member 44 shown in FIGS. 3-7 are not intended to be limiting. Any suitable shapes or mechanisms may be utilized that allow for expansion of the valve support structure 42, such as sinusoidal, accordion, triangular or any combination of segments and/or arcuate shapes.

[0050] It is noted that the gap in the sewing ring 46 shown in FIGS. 4, 5, and 7, for example, is provided in the Figures for illustrative purposes. Such a gap would not typically be provided, although it is contemplated that such sewing ring 46 does include such a gap. When the base portion of the sewing ring 46 includes such a gap, cloth or another material that is used to cover the rest of the sewing ring 46 would preferably span such a gap to provide a continuous cover around the perimeter of the sewing ring 46. In this way, the paravalvular seal can be maintained more easily once the device is implanted in a patient. This material may be stretchable or otherwise deformable to allow for expansion of the overall size of the valve, if desired. If the sewing ring 46 does not include a gap, the ring 46 can be expandable or deformable, such as can be accomplished with a deformable material (e.g., stretchable portions) and/or with one or more expandable portions.

[0051] FIG. 3 further illustrates an optional restraining element 48 that is positioned around a portion of one of the members 44. In this embodiment, support structure 42 can be a self-expanding component, where element 48 is positioned in such a way that it maintains the member 44 in an initial or unexpanded condition. The restraining element 48 can later be removed, deformed, or broken in order to allow the member 44 to deform or straighten, thereby allowing overall support structure 42 to expand to a larger diameter. One or more restraining elements 48 can be positioned relative to some or all of the members 44, wherein if more than one restraining element is used, the number of elements 48 that are deformed or removed can be chosen to allow the desired amount of expansion of the support structure 42. That is, only one element 48 may be removed in a first procedure to allow a first amount of expansion of the support structure 42, and then one or more additional elements 48 can be removed in one or more subsequent procedures to allow additional expansion of the support structure 42.

[0052] The valve support structure can also be composed of multiple elements that function together in a similar manner as a single valve support structure of the type previously described. For one example, the valve support structure may include an outer tubular structural piece having a central opening into which a connector can be positioned. Such a connector can be slideable relative to the outer tubular structural piece to allow for expansion of the outer periphery of the support structure. In another embodiment, tracks or rails can be used to allow for enlargement or expansion of the outer perimeter of the support structure.

[0053] A portion of a post-implant expansion system 50 is illustrated in FIG. 7, which comprises an expandable member 52 (e.g., a balloon that can be made of nylon, polyurethane, polyethylene, or polyethylene terephthalate (PET)). The system 50 may be utilized to modify the valve structure 40 from its first, unexpanded or partially expanded position to its second, expanded or partially expanded position. When the assembly 10 and valve structure 40 are in their second, expanded positions or configurations, they may be configured to receive a replacement transcatheter valve assembly. For example, a replacement valve conduit may be placed between the balloon 22 and the inside of the expandable conduit 14 in FIG. 2. In this embodiment, the assembly 10 is enlarged to its expanded condition and a replacement valve can be subsequently or simultaneously implanted therein. The native or existing valve can serve as a landing zone for a new heart valve implant. It is also possible to first expand the valve structure and to later insert a replacement transcatheter valve, where this can be performed either a relatively short time or a relatively long time after that expansion is performed.

[0054] FIGS. 8 and 9 illustrate another conduit configuration that can be used with certain aspects of the invention. In particular, a conduit 60 is illustrated in FIG. 8, which may comprise a specially designed expandable structure 62. This conduit 60 may or may not include a valve, depending on the application. In the depicted embodiment, the structure 62 comprises a mesh or woven type of material configuration (e.g., a biocompatible polymer, metal, or combination thereof). The expandable structure 62 may comprise multiple members 66 disposed between adjacent elongated member 68, shown in FIG. 9, which can withstand stresses and tension during expected use of the heart valve assembly. However, the members 66 are designed to permanently deform, stretch, and/or break under the applied load of an expandable balloon

member (not shown in FIGS. 8 and 9) or another device that imparts radial force. These members 66 may be fabric fibers, wires, or polymer elements, for example, which can break or stretch when placed under stress. If the members 66 stretch, such a stretching will preferably cause permanent or semi-permanent deformation of the members 66 so that they do not contract all the way back to their original size once the stress or load is removed. Members 64 are longer than members 66 and are curved or bent when the conduit 60 is in its relatively unexpanded condition. In addition, members 64 are more robust and are designed to withstand more stress than members 66. As a result, when a balloon or other expandable member is placed within the structure 62 and expanded, the members 66 will break or stretch and the members 64 will become straighter, thereby affording expansion of the expandable conduit 60. Members 66 can be differently configured at various portions of the conduit (e.g., inflow, outflow, etc.) to allow various shapes upon application of loads.

[0055] FIGS. 10-12 schematically illustrate a surgical method according to the invention. Specifically, FIG. 10 shows an aortic annulus 102, which may be relatively small, either due to the patient's natural anatomy or excessive calcification. An implantable valve 100 according to the invention is implanted in the patient's vasculature 104 (e.g., encompassing the native valve or occupying the position of a removed valve). Prior to this step, a sizing balloon or surgical valve sizer can be utilized to identify a desired maximum size of the valve 100.

[0056] A valve can be relative easily sewn into the patient's anatomy in the condition illustrated in FIG. 10. FIG. 11 then shows the use of a balloon 110 to expand the valve 100 to a larger circumference, which can be performed at any time after the initial valve implantation. FIG. 12 shows the valve 100' after it has been enlarged to an expanded condition. In this manner, the present invention can be utilized to maximize the effective valve orifice for a particular patient following the initial implantation procedure.

[0057] In another surgical embodiment, an expandable bioprosthetic valve may be implanted in the patient in an unexpanded, yet functional condition. That valve may be used until the useful life of its components reach an endpoint or the patient outgrows it. In this embodiment, an expandable member may then be utilized to modify or enlarge the valve to its expanded condition, and then a replacement transcatheter valve (which may itself be expandable) may be implanted with the first bioprosthetic valve. In this way, larger orifice areas following transcatheter valve procedures may be available than would be available with conventional surgical valves.

[0058] FIGS. 13-15 illustrate another embodiment of a component 200 of the invention. The component 200 comprises a tubular conduit 204 with at least two releasable seams 202, although it is possible that component 200 comprises more or less than two seams. The releasable seams 202 are positioned to essentially create a loop 206 of material from a tubular structure, where the seam 202 is sewn or otherwise secured (e.g., clips, sutures, and the like) along a seam line. When desired, the conduit 204 can be loaded radially, thereby breaking, deforming, stretching, or otherwise releasing material of the seams 202 (i.e., the loop 206) and allowing the component 200 to expand. That is, all or most of the material that makes up the loop 206 will be exposed to the inner area of the conduit 204 after expansion of the component 200. As shown in FIG. 15, the seam 202 may be created with a series

of breakable or stretchable fibers (e.g., fabric fibers, wires, or polymeric elements), or discrete deformable elements 205 that can be broken or deformed by the application of a radial force, such as by a balloon expandable member. Although the loop 206 is shown on the exterior of the component 200 in FIG. 13, it may alternatively be placed within the interior area of the component 200.

[0059] FIGS. 16 and 17 illustrate a portion of another embodiment of a seam of a tubular conduit, which includes a series of discrete deformable elements 207, one of which is illustrated in these figures. Element 207 is shown in its unexpanded condition in FIG. 16 as having a diameter or dimension d1, then in its expanded condition in FIG. 17 as having a diameter or dimension d2. Diameter d1 is at least somewhat smaller than the diameter d2, which thereby illustrates the expansion in the seam area of the conduit. This deformation of the element 207 is preferably permanent or semi-permanent after the force that was used to deform the element is removed. Similarly, FIGS. 21 and 22 illustrate another deformable element 214. Element 214 is shown in its unexpanded condition in FIG. 21 as having a width or length d1, then in its expanded condition in FIG. 22 as having a width or length d2. Dimension d1 is smaller than the dimension d2, which again illustrates the expansion of the seam area of the conduit.

[0060] FIGS. 18-20 illustrate a portion of another embodiment of a loop 206 of a conduit seam, and further including a deformable element 208. Deformable element 208 includes lobes 212 and a bar 210 extending from each lobe 212. The lobes 212 are spaced from each other around the element 208. As is best illustrated in FIG. 19, material of the conduit 204 is looped relative to the bars 210 to create the loop of a seam. Application of radial force, such as the expansion of an internally positioned balloon, can deform the element 208, thereby allowing expansion of the seam.

[0061] The present invention has now been described with reference to several embodiments thereof. The entire disclosure of any patent or patent application identified herein is hereby incorporated by reference. The foregoing detailed description and examples have been given for clarity of understanding only. No unnecessary limitations are to be understood therefrom. It will be apparent to those skilled in the art that many changes can be made in the embodiments described without departing from the scope of the invention. Thus, the scope of the present invention should not be limited to the structures described herein, but only by the structures described by the language of the claims and the equivalents of those structures.

What is claimed is:

1. A prosthetic heart valve comprising:
 - a valved conduit comprising a generally tubular structure having at least one leaflet attached within its interior area;
 - a plurality of support structures connected to the tubular structure and spaced from each other along a length of the tubular structure, wherein each of the support structures is expandable from a first configuration to a second configuration when subjected to internal radial stress, wherein the internal area of each support structure is smaller in its first configuration than in its second configuration.
2. The heart valve of claim 1, wherein each of the support structures is attached to an outer surface of the tubular structure.

3. The heart valve of claim 1, wherein each of the support structures are attached within the interior area of the tubular structure.

4. The heart valve of claim 1, wherein each of the support structures are embedded within an outer wall of the tubular structure.

5. The heart valve of claim 1, wherein the heart valve is surgically implantable in a patient with the support structures in their first configuration, and wherein the support structures are expandable to their second configuration in response to the application of radial stress by a separate radial expansion system.

6. The heart valve of claim 1, wherein the first configuration of each of the support structures comprises a shaped portion, and wherein the shaped portion of the support structures is at least partially straightened when the support structure is in its second configuration.

7. The heart valve of claim 1, wherein the tubular structure has a central area having a smaller diameter than a diameter of at least one of a first end and a second end of the tubular structure.

8. The heart valve of claim 7, wherein the at least two leaflets are attached within the central area of the tubular structure.

9. A prosthetic heart valve comprising:

a sewing ring from which a plurality of stent posts extend, wherein the sewing ring is a generally tubular structure that is expandable from a first configuration to a second configuration, wherein an internal area of the sewing ring is smaller in its first configuration than in its second configuration;

at least one leaflet attached within an interior area of the sewing ring; and

a reconfigurable support structure, wherein at least a portion of the support structure is attached to at least one of the stent posts.

10. The heart valve of claim 9, wherein the support structure is reconfigurable from a first configuration to a second configuration when the sewing ring is subjected to internal radial stress, wherein the internal area of the support structure is smaller in its first configuration than in its second configuration.

11. The heart valve of claim 9, wherein the sewing ring comprises a frame having a gap that is smaller when the sewing ring is in its first configuration than when the sewing ring is in its second configuration, and wherein the frame and the gap are covered by a flexible covering material.

12. The heart valve of claim 11, wherein the flexible covering material surrounds the sewing ring, stent posts, and gap.

13. The heart valve of claim 11, wherein the support structure is a self-expanding structure.

14. The heart valve of claim 13, further comprising at least one restraining member positioned to compress a portion of the support structure to maintain the support structure in its first configuration.

15. A prosthetic heart valve comprising a valved conduit comprising a generally tubular structure having at least one leaflet attached within its interior area, wherein the tubular structure comprises:

a plurality of longitudinal support members spaced from each other around the perimeter of the tubular structure; at least one deformable member attached at a first end to a first longitudinal support member and at a second end to an adjacent second longitudinal support member, wherein the at least one deformable member is reconfigurable when the tubular structure is subjected to an internal radial stress.

16. The heart valve of claim 15, wherein the at least one deformable member is permanently deformable.

17. The heart valve of claim 15, wherein the at least one deformable member is breakable.

18. The heart valve of claim 15, further comprising at least one connector member attached at a first end to the first longitudinal member and at a second end to the second longitudinal member, wherein the at least one connector member has a higher strength than a strength of the at least one deformable member such that when the tubular structure is subjected to an internal radial stress, the at least one deformable member will deform by a sufficient amount that the distance between the first and second longitudinal support members will increase and such that the connector member will remain attached to the first and second longitudinal support members.

19. A prosthetic heart valve comprising a valved conduit comprising a generally tubular structure having a length extending along a longitudinal axis, wherein the tubular structure comprises:

a first seam extending along at least a portion of the length of the tubular structure; and

a second seam spaced from the first seam and extending along at least a portion of the length of the tubular structure;

wherein the first and second seams are positioned relative to each other to form a loop of material that reduces an internal diameter of the tubular structure from an expanded configuration to a compressed configuration.

20. The prosthetic heart valve of claim 19, wherein the first and second seams are releasable to allow expansion of the tubular structure from its compressed configuration to its expanded configuration.

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