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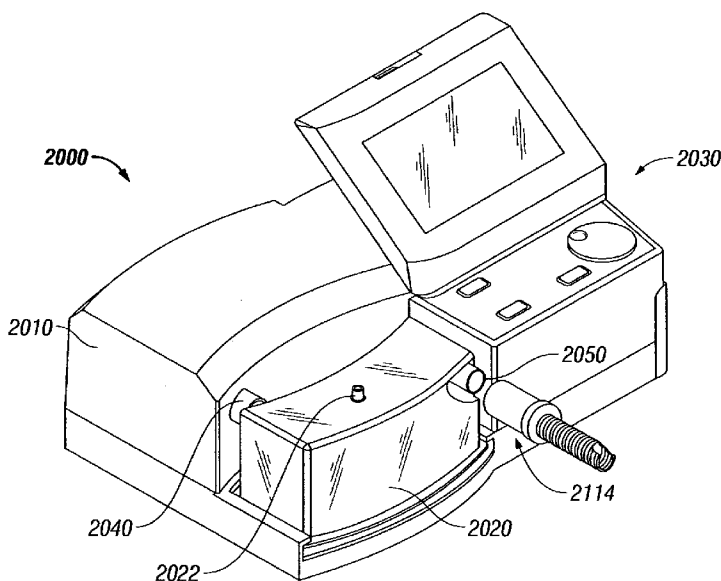
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(57) Abstract: A high flow therapy system including a microprocessor, a heating element a non-sealing respiratory interface and a sensor is disclosed. The heating element is disposed in electrical communication with the microprocessor and is capable of heating a liquid to create a gas. The non-sealing respiratory interface is configured to deliver the gas to a patient. The sensor is disposed in electrical communication with the microprocessor and is configured to measure pressure in an upper airway of the patient.

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**HIGH FLOW THERAPY DEVICE UTILIZING A NON-SEALING
RESPIRATORY INTERFACE AND RELATED METHODS**

CORRESPONDING PRIOR US NATIONAL APPLICATION

[0001] This application corresponds to prior US national application serial no. [not yet known], entitled "High Flow Therapy Device Utilizing A Non-Sealing Respiratory Interface And Related Method" filed on December 6, 2007 by Charles A. Lewis et al. under US Mail Label Number EM 109 151 867 US (Application Docket No. 1573-6 CIP). The entire contents of which are hereby incorporated by reference herein.

CROSS-REFERENCE TO RELATED APPLICATIONS

[0002] This application relates to U.S. Patent Application Serial No. 11/638,981, filed on December 14, 2006 (1573-6). This application also relates to PCT International Application No. PCT/US2006/047640, entitled "High Flow Therapy Device Utilizing A Non-Sealing Respiratory Interface And Related Method" filed on December 14, 2006. The entire contents of these applications are hereby incorporated by reference herein.

BACKGROUND

[0003] Respiratory interfaces, e.g., nasal cannulas are used to deliver respiratory gases for therapeutic effect, including oxygen therapy, treatment for sleep apnea, and respiratory support. Small nasal cannulas are commonly used for delivery of low volumes of oxygen. Sealing nasal cannulas, such as the cannulas disclosed in U.S. Patent No. 6,595,215 to Wood, are used for the treatment of sleep apnea. However, treatment with certain types of nasal cannulas may be limited by the lack of

information available on important treatment parameters. These parameters include information regarding the gases within the user's upper airway, such as pressure, flow rate, and carbon dioxide build up. These and other data may be useful in judging the efficacy of treatment as well as for controlling and monitoring treatment.

[0004] In addition, prior art nasal cannula designs (especially those designed for neonatal oxygen therapy) may undesirably create a seal with the user's nares, which may have detrimental effects on the user's health.

[0005] Oxygen (O₂) therapy is often used to assist and supplement patients who have respiratory impairments that respond to supplemental oxygen for recovery, healing and also to sustain daily activity.

[0006] Nasal cannulas are generally used during oxygen therapy. This method of therapy typically provides an air/gas mixture including about 24% to about 35% O₂ at flow rates of 1-6 liters per minute (L/min). At around two liters per minute, the patient will have an FiO₂ (percent oxygen in the inhaled O₂/air mixture) of about 28% oxygen. This rate may be increase somewhat to about 8 L/min if the gas is passed through a humidifier at room temperature via a nasal interface into the patient's nose. This is generally adequate for many people whose condition responds to about 35-40% inhaled O₂ (FiO₂), but for higher concentrations of O₂, higher flow rates are generally needed.

[0007] When a higher FiO₂ is needed, one cannot simply increase the flow rate. This is true because breathing 100% O₂ at room temperature via a nasal cannula is irritating to the nasal passage and is generally not tolerated above about 7-8 L/min. Simply increasing the flow rate may also provoke bronchospasm.

[0008] To administer FiO₂ of about 40% to about 100%, non-re-breathing masks (or sealed masks) are used at higher flows. The mask seals on the face and has a

reservoir bag to collect the flow of oxygen during the exhalation phase and utilize one-way directional valves to direct exhalation out into the room and inhalation from the oxygen reservoir bag. This method is mostly employed in emergency situations and is generally not tolerated well for extended therapy.

[0009] High flow airway respiratory support (“high flow therapy” or “HFT”) is administered through a nasal cannula into an “open” nasal airway. The airway pressures are generally lower than Continuous Positive Airway Pressure (CPAP) and Bi-level Positive Airway Pressure (BiPAP) and are not monitored or controlled. The effects of such high flow therapies are reported as therapeutic and embraced by some clinicians while questioned by others because it involves unknown factors and arbitrary administration techniques. In such procedures, the pressures generated in the patients’ airways are typically variable, affected by cannula size, nare size, flow rate, and breathing rate, for instance. It is generally known that airway pressures affect oxygen saturation, thus these variables are enough to keep many physicians from utilizing HFT.

SUMMARY

[0010] The present disclosure relates to a high flow therapy system including a microprocessor, one or more heating elements, a non-sealing respiratory interface and a sensor. The heating elements are disposed in electrical communication with the microprocessor and is capable of heating a liquid to create a gas. The non-sealing respiratory interface is configured to deliver the gas to a patient. The sensor is disposed in electrical communication with the microprocessor and is configured to measure pressure in an upper airway of the patient.

[0011] The present disclosure also relates to a method of supplying a patient with gas. The method includes providing a high flow therapy device including a microprocessor, one or more heating elements disposed in electrical communication with the microprocessor and capable of heating a liquid to create a gas, a non-sealing respiratory interface configured to deliver the gas to a patient and a sensor disposed in electrical communication with the microprocessor and configured to measure pressure in the upper airway of the patient. This method also includes heating the gas and delivering the gas to a patient.

[0012] The present disclosure also relates to a method of minimizing respiratory infections of a patient. The method includes providing a high flow therapy device, heating the gas and delivering the gas to a patient. The high flow therapy device of this method includes at least one heating element capable of heating a liquid to create a gas and a non-sealing respiratory interface configured to deliver the gas to a patient.

[0013] The present disclosure also relates to a method of supplying a patient with gas. The method including providing a high flow therapy device, heating a gas and delivering the gas to a patient. The high flow therapy device of this method includes at least one heating element, a non-sealing respiratory interface, a blower, an air inlet port and an air filter. The at least one heating element is capable of heating a liquid to create a gas. The non-sealing respiratory interface is configured to deliver the gas to a patient. The blower is disposed in mechanical cooperation with the non-sealing respiratory interface and is capable of advancing the gas at least partially through the non-sealing respiratory interface. The air inlet port is configured to enable ambient air to flow towards to the blower. The air filter is disposed in mechanical cooperation with the air inlet port and is configured to remove particulates from the ambient air.

[0014] The present disclosure also relates to a method of supplying a patient with gas. The method includes providing a high flow therapy device, heating a gas and delivering the gas to a patient. The high flow therapy device of this method includes at least one heating element, a non-sealing respiratory interface, and controlling a source of one or more compressed gases. The at least one heating element is capable of heating a liquid to create a gas. The non-sealing respiratory interface is configured to deliver the gas to a patient. The compressed gas control mechanism is disposed in mechanical cooperation with the non-sealing respiratory interface and is capable of advancing the gas at least partially through the non-sealing respiratory interface.

[0015] The present disclosure also relates to a method of treating a patient for an ailment such as a headache, upper airway resistance syndrome, obstructive sleep apnea, hypopnea and snoring. The method includes providing a high flow therapy device, heating a gas and delivering the gas to a patient. The high flow therapy device includes at least one heating element capable of heating a liquid to create a gas and a non-sealing respiratory interface configured to deliver the gas to a patient.

[0016] The present disclosure also relates to a method of delivering respiratory gas to a patient. The method includes providing a high flow therapy device, monitoring the respiratory phase of the patient and pressurizing the gas. The high flow therapy device of this method includes at least one heating element capable of heating a liquid to create a gas, a non-sealing respiratory interface configured to deliver the gas to a patient, and a sensor configured to measure pressure in the upper airway of the patient.

[0017] The present disclosure also relates to a high flow therapy device including a microprocessor, at least one heating element, a non-sealing respiratory interface, a sensor and a mouthpiece. The at least one heating element is disposed in electrical

communication with the microprocessor and is capable of heating a liquid to create a gas. The non-sealing respiratory interface is configured to deliver the gas to a patient. The sensor is disposed in electrical communication with the microprocessor and is configured to measure pressure in an upper airway of the patient. The mouthpiece is disposed in mechanical cooperation with the sensor.

BRIEF DESCRIPTION OF THE DRAWINGS

[0018] Reference will now be made to the accompanying drawing figures, which are not necessarily drawn to scale.

[0019] Figure 1 is a perspective view of a nasal cannula according to a particular embodiment of the invention.

[0020] Figure 2 is a perspective view of a nasal cannula according to a further embodiment of the invention.

[0021] Figure 3 is a perspective view of a nasal cannula according to another embodiment of the invention.

[0022] Figure 4 is a perspective view of a nasal cannula according to yet another embodiment of the invention.

[0023] Figure 5 is a front perspective view of a nasal cannula according to a further embodiment of the invention.

[0024] Figure 6 depicts a cross section of a nasal insert of a nasal cannula according to a particular embodiment of the invention.

[0025] Figure 7 depicts a cross section of a nasal insert of a nasal cannula according to a further embodiment of the invention.

[0026] Figure 8A is a front perspective view of a nasal cannula according to another embodiment of the invention.

[0027] Figure 8B is a rear perspective view of the nasal cannula shown in Figure 8A.

[0028] Figure 8C is a perspective cross-sectional view of the nasal cannula shown in Figure 8A.

[0029] Figure 9 is a perspective view of a nasal cannula according to a further embodiment of the invention.

[0030] Figure 10 is a perspective view of a nasal cannula according to another embodiment of the invention.

[0031] Figure 11 is a perspective view of a nasal cannula according to a further embodiment of the invention.

[0032] Figure 12 is a perspective view of a nasal cannula according to yet another embodiment of the invention.

[0033] Figure 13 illustrates an embodiment of a nasal cannula in use on a patient, according to one embodiment of the invention.

[0034] Figure 14 illustrates another embodiment of a nasal cannula in use on a patient, according to a further embodiment of the invention.

[0035] Figure 15 illustrates a perspective view of a high flow therapy device in accordance with an embodiment of the present disclosure.

[0036] Figure 16 illustrates a perspective view of the high flow therapy device of Figure 15 showing internal components, in accordance with an embodiment of the present disclosure.

[0037] Figures 17 and 17A illustrates a schematic view of the high flow therapy device of Figures 15 and 16 with a nasal interface and a patient in accordance with embodiments of the present disclosure.

[0038] Figure 18 illustrates a high flow therapy device including a nasal interface and a conduit in accordance with an embodiment of the present disclosure.

[0039] Figures 19 and 20 illustrate an enlarged view of a patient's upper airway and a nasal interface in accordance with two embodiments of the present disclosure.

[0040] Figure 21 illustrates an example of a screen shot of a user interface of the high flow therapy device of Figures 15-17 in accordance with an embodiment of the present disclosure.

[0041] Figures 22 and 23 illustrate examples of a non-sealing respiratory interface in the form of a mouthpiece in accordance with embodiments of the present disclosure.

[0042] Figure 24 illustrates a mouthpiece of Figures 22 or 23 in use on a patient in accordance with an embodiment of the present disclosure.

[0043] Figure 25 illustrates an enlarged view of a connector according to an embodiment of the present disclosure.

[0044] Figure 26 illustrates a perspective view of a therapy device and the connector of Figure 25.

[0045] Figure 27 illustrates a longitudinal cross-sectional view of the connector of Figures 25 and 26.

[0046] Figure 28 illustrates a top view of the therapy device of Figure 26 having the connector operably coupled to the therapy device.

[0047] Figure 29 is a transverse cross-sectional view of a humidity chamber of a therapy device according to an embodiment of the present disclosure.

[0048] Figures 29A-29C are an enlarged sectional views of a portion of the humidity chamber according to embodiments of the present disclosure.

[0049] Figure 30 is a perspective view of a connector according to an embodiment of the present disclosure.

[0050] Figure 31 is a longitudinal cross-sectional view of the connector of Figure 30.

[0051] Figures 32A and 32B are schematic illustrations of the flow of gas according to embodiments of the present disclosure.

[0052] Figures 33A-33C show various aspects of a humidity chamber in accordance with embodiments of the present disclosure.

[0053] Figures 34A-34D illustrate a saddle for use with a therapy device of the present disclosure.

[0054] Figure 35 illustrates a patient with a nasal cannula and an ear lobe probe.

DETAILED DESCRIPTION

[0055] The present inventions now will be described with reference to the accompanying drawings, in which some, but not all embodiments of the inventions are shown. Indeed, these inventions may be embodied in many different forms and should not be construed as limited to the embodiments set forth herein. Rather, these embodiments are provided so that this disclosure will satisfy applicable legal requirements. Like numbers refer to like elements throughout. For example, elements **130**, **230**, **330**, **430**, **530**, **830**, and **930** are all nasal inserts according to various embodiments of the invention.

[0056] Overview of Functionality

[0057] Nasal cannula according to various embodiments of the invention may be configured to deliver high-flow therapeutic gases to a patient's upper airway through

the patient's nose. Such gases may include, for example, air, humidity, oxygen, therapeutic gases or a mixture of these, and may be heated or unheated. In particular embodiments of the invention, the cannula may be useful for CPAP (continuous positive airway pressure) applications, which may be useful in the treatment of sleep apnea and in providing respiratory support to patients (e.g., after abdominal surgery), to alleviate snoring, or for other therapeutic uses.

[0058] Nasal cannula according to particular embodiments of the invention include (or are adapted to facilitate the positioning of) one or more sensors adjacent or within one or more of the cannula's nasal inserts. Accordingly, the nasal cannula may be configured so that at least a portion of one or more sensors is in place in one or both of a user's nares when the nasal cannula is operably worn by the user. This may be particularly helpful in evaluating the environment of the internal portion of the user's nose and/or the user's upper airway. As described in greater detail below, in various embodiments of the invention, the cannula is adapted so that it will not create a seal with the patient's nares when the cannula is in use.

[0059] Nasal cannula according to other embodiments of the invention include nozzles that are adapted to remain outside of a user's nares while the cannula is in use. Accordingly, the nozzles avoid sealing with the patient's nares while the cannula is in use. In some embodiments, the nasal cannula include elongate extensions that are inserted into the user's nares to detect pressure in one or both nares.

[0060] In certain embodiments of the invention, sensors are provided adjacent or within both of the nasal cannula's nasal inserts. In various other embodiments, sensors are provided adjacent or within one or more elongate extensions that extend into the user's nares. In various embodiments, elongate extensions may be used in conjunction with nasal inserts or with nozzles. The use of sensors may be useful, for

example, in monitoring environmental changes from one of the user's nares to the other. This information may be helpful, for example, in determining when the dominant flow of air changes from one of the user's nares to the other, which may affect the desired flow characteristics of therapy. Accordingly, data from each nare may provide information which may be useful in establishing or modifying the user's treatment regimen. Further, multiple sensors may be used in various embodiments.

[0061] Overview of Exemplary Cannula Structures

[0062] A cannula **100** according to one embodiment of the invention is shown in Figure 1. As may be understood from this figure, in this embodiment, the cannula **100** includes a hollow, elongated tubular base portion **105** that includes a central portion **110**, a first end portion **115**, and a second end portion **120**. The first and second end portions **115**, **120** may be angled relative to the central portion **110** as shown in Figure 1.

[0063] In various embodiments of the invention, the cannula **100** includes a first inlet **117** adjacent the outer end of the first end portion **115**, and a second inlet **122** adjacent the second end portion **120** (in other embodiments, the cannula may include only one such inlet). The cannula **100** further comprises a pair of hollow, elongated, tubular nasal inserts (e.g., nasal catheters) **125**, **130** that extend outwardly from the nasal cannula's base portion **105** and that are in gaseous communication with the base portion's interior. In various embodiments, the respective central axes of the nasal inserts **125**, **130** are substantially parallel to each other, and are substantially perpendicular to the central axis of the central portion **110** of the nasal cannula's base portion **105**.

[0064] In particular embodiments of the invention, the cannula defines at least one conduit that is adapted to guide at least one sensor so that the sensor is introduced adjacent or into the interior of the cannula so that, when the cannula is being operably worn by a user, the environment being monitored by the at least one sensor reflects that of the internal portion of the user's nose and/or the user's upper airway. In various embodiments of the invention, a user may temporarily insert the at least one sensor into or through the conduit to determine correct settings for the cannula system, and then may remove the sensor after the correct settings have been achieved. In other embodiments, the at least one sensor may be left in place within the conduit for the purpose of monitoring data within (or adjacent) the cannula over time (e.g., for purposes of controlling the user's therapy regimen). In a further embodiment, the at least one sensor may be positioned adjacent an outlet of the conduit.

[0065] The at least one sensor may be connected (e.g., via electrical wires) to a computer and/or a microprocessor that is controlling the flow of respiratory gases into the cannula. The computer may use information received from the at least one sensor to control this flow of gas and/or other properties of the system, or may issue an alarm if the information satisfies pre-determined criteria (e.g., if the information indicates potentially dangerous conditions within the patient's airway or if the system fails to operate correctly).

[0066] As may be understood from Figures 8A–8C, in a particular embodiment of the invention, at least one of the cannula's conduits **850** is defined by, and extends within, a side wall of the cannula **800**. Alternatively, the conduit may be disposed within an interior passage defined by the cannula. For example, one or more of the conduits may be defined by a tube that is attached immediately adjacent an interior surface of the cannula (e.g., adjacent an interior surface of the cannula's base portion,

or an interior surface of one of the cannula's nasal inserts). The cannula's conduits are preferably adapted for: (1) receiving a flow of gas at one or more inlets that are in communication with the conduit, and (2) guiding this flow of gas to an outlet in the cannula. In various embodiments, one or more of the inlets is defined within an exterior portion of one of the cannula's nasal inserts.

[0067] As may be understood from Figure 1, in various embodiments of the invention, each of the cannula's conduit outlets **136, 141** is located at the end of a respective elongate, substantially tubular, outlet member **135, 140**. For example, in the embodiment shown in Figure 1, the cannula **100** includes a first outlet member **135** that is substantially parallel to the cannula's first nasal insert **125**. In this embodiment, the first outlet member **135** and the first nasal insert **125** may be positioned on opposite sides of the nasal cannula's base portion **105** as shown in Figure 1. Similarly, in a particular embodiment of the invention, the cannula **100** includes a second outlet member **140** that is substantially parallel to the cannula's second nasal insert **130**. The second outlet member **140** and second nasal insert **130** are also preferably positioned on opposite sides of the nasal cannula's base portion **105**.

[0068] In various embodiments of the invention, a sensor (e.g., a pressure, temperature, or O₂ sensor) is provided adjacent at least one of (and preferably each of) the cannula's outlets **136, 141** and is used to measure the properties of gas from that outlet **136, 141**. In a further embodiment of the invention, accessory tubing is used to connect each outlet **135, 140** with at least one corresponding sensor (and/or at least one external monitoring device) that may, for example, be spaced apart from the cannula **100**.

[0069] In yet another embodiment of the invention, one or more sensors are provided within the conduit, and used to measure the properties of gas accessed through the conduit. In this embodiment, information from each sensor may be relayed to a control system outside the cannula via, for example, an electrical wire that extends from the sensor and through the outlet **135, 140** of the conduit in which the sensor is disposed.

[0070] In alternative embodiments of the invention, each of the cannula's conduits may extend: (1) from the inlets **152, 154**; (2) through, or adjacent, a side wall of one of the cannula's nasal inserts **125, 130**; (3) through, or adjacent, a side wall of the cannula's body portion **105**; and (4) to an outlet **135, 140** that is defined within, or disposed adjacent, the cannula's body portion **105**. In one such embodiment, the conduit comprises a substantially tubular portion that is disposed adjacent an interior surface of the cannula's body portion.

[0071] As may be understood from Figure 2, in certain embodiments of the invention, the cannula **200** includes at least one sensor **245** that is integrated into an exterior portion of the cannula **200** (e.g., within a recess **223** formed within an exterior surface of one of the cannula's nasal inserts **225, 230**). In this embodiment, information from the sensor **245** may be relayed to a control system outside the cannula **200** via an electrical wire **246** that extends from the sensor **245**, through a conduit, and out an outlet **235, 240** in the conduit. In various embodiments of the invention, the conduit extends through or adjacent an interior portion of a side wall of one of the cannula's nasal inserts **225, 230** and/or through or adjacent an interior portion of a side wall of the cannula's body portion **205**.

[0072] In particular embodiments of the invention, at least one sensor **245** is fixedly attached to the cannula **100** so that it may not be easily removed by a user.

Also, in particular embodiments, at least one sensor **245** is detachably connected adjacent the cannula **100** so that the sensor **245** may be easily detached from (and, in certain embodiments, reattached to) the cannula **100**.

[0073] The cannula **1000** includes a hollow, elongated tubular base portion **1005** that includes a central portion **1010**, a first end portion **1015**, and a second end portion **1020**. The first and second end portions **1010**, **1015** may be angled relative to the central portion **1010**, as shown in Figure 10. In various embodiments of the invention, the cannula **1000** includes a first inlet **1017** adjacent the outer end of the first end portion **1015**, and a second inlet **1022** adjacent the outer end of the second end portion **1020**.

[0074] The cannula **1000** further comprises a pair of hollow, elongated, tubular nozzles (a first nozzle **1026** and a second nozzle **1031**) that extend outwardly from the nasal cannula's base portion **1005**. In various embodiments, the respective central axes of the nozzles **1026**, **1031** are substantially parallel to each other and are substantially perpendicular to the central axis of the central portion **1010** of the nasal cannula's base portion **1005**. In various embodiments, the nozzles **1026**, **1031** define conduits that are in gaseous communication with the interior of the cannula's base portion **1005**. In particular embodiments of the invention, the first and second nozzles **1026**, **1031** are adapted to be positioned outside of a user's nares while the cannula is in use. In particular embodiments, the nozzles **1026**, **1031** each define a respective nozzle outlet. For example, the first nozzle **1026** defines a first nozzle outlet **1083**, and the second nozzle **1031** defines a second nozzle outlet **1084**. In various embodiments, when the nasal cannula **1000** is operatively positioned adjacent a user's nares, each of the nozzle's outlets **1083**, **1084** is positioned to direct a focused flow of gas into a corresponding one of the user's nares.

[0075] In alternative embodiments, such as the embodiment shown in Figure 12, the nasal cannula **1200** may include a single nozzle **1227** that defines a conduit or air passageway that is in gaseous communication with an interior portion of the cannula's base portion **1205**. As described in greater detail below, in various embodiments, the nozzle **1227** extends outwardly from the cannula's base portion **1205** and has an oblong, or elliptical, cross-section. In this and other embodiments, the nozzle **1227** is shaped to deliver a focused flow of gas simultaneously into both of a user's nares when the cannula **1200** is in use.

[0076] In various embodiments, the nasal cannula includes one or more elongate extensions that are adapted for insertion into one or more of the user's nares. For example, returning to the embodiment shown in Figure 10, the nasal cannula **1000** may include multiple elongate extensions (for example a first elongate extension **1070** and a second elongate extension **1072**) that are long enough to allow each of the elongate extensions **1070**, **1072** to be inserted into a respective one of the user's nares while the nasal cannula **1000** is in use. In various embodiments, each of the elongate extensions **1070**, **1072** may have a central axis that runs substantially parallel to the central axis of a corresponding nozzle **1026**, **1031**. For example, as can be understood from Figure 10, in certain embodiments, a first elongate extension **1070** has a central axis that lies substantially parallel to and below the central axis of a corresponding first nozzle **1026**, when the nasal cannula is operatively positioned adjacent a user's nares. Similarly, in various embodiments, a second elongate extension **1072** has a central axis that lies substantially parallel to and below the central axis of a corresponding second nozzle **1031**, when the nasal cannula **1000** is operatively positioned adjacent a user's nares. In various other embodiments, the elongate

extensions may lie within, and extend outwardly from, their corresponding nozzles **1070, 1072**.

[0077] As a further example, Figure 12 illustrates an exemplary nasal cannula **1200** having multiple elongate extensions (a first elongate extension **1270** and a second elongate extension **1272**), which both lie substantially below a single nozzle **1227** when the nasal cannula **1200** is in an operative position adjacent the user's nose. In some embodiments, the central axes of the first and second elongate extensions **1270, 1272**, may be substantially parallel to the central axis of the nozzle **1227**. Also, in various embodiments, one or both of the elongate extensions **1270, 1272** may lie within the nozzle **1227**. In this and other embodiments, a distal end of each of the elongate extensions **1270, 1272** may extend beyond a distal end of the nozzle **1227**.

[0078] As described above, in certain embodiments of the invention, the nasal cannula includes one or more sensors that are adapted to measure gas data (e.g., gas pressure) within the user's nares while the nasal cannula is in use. For example, the nasal cannula **1000** shown in Figure 10 may include a sensor positioned adjacent the distal end of one or both of the first and second elongate extensions **1070, 1072**. In various embodiments, each elongate extension may be adapted to: (1) support a sensor adjacent (e.g., at) the distal end of the elongate extension; and (2) support a wire that is simultaneously connected to the sensor and a control mechanism that is adapted to adjust the properties of gas flowing through the cannula **1000**.

[0079] In other embodiments, the elongate extensions define conduits. For example, the sensor(s) may be positioned within the interior or exterior of the elongate extensions and information from the sensor(s) may be relayed to a control system via a wire extending through a conduit (for example, conduit **1023** of Figure 10) or passageway defined by each of the elongate extensions. In one embodiment, as

shown, for example, in Figure 10, the conduit **1023** is shaped similarly to the nasal cannula's base portion **1005**, and lies substantially below the base portion **1005** when the nasal cannula **1000** is operatively in use. In various embodiments, the conduit **1023** is positioned within the base portion **1005** such that the first and second elongate extensions **1070**, **1072** lie within, and extend outwardly from, the respective first and second nozzles **1026**, **1031**.

[0080] In various embodiments, each elongate extension defines a respective conduit that can serve as an air passageway. For example, in certain embodiments, each conduit is adapted to provide a passage that permits gaseous communication between a user's nares and a control system or other device for measuring and adjusting the properties of the air. In this and other embodiments, a sensor may be positioned at the control box to measure the properties (e.g., pressure) of air in the user's nares. In some embodiments, the elongate extensions define a conduit that serves both as an air passageway as well as a conduit for allowing a wire to pass from a sensor positioned adjacent the tip of the elongate extension to the control system or other device.

[0081] Data Monitored by Sensors

[0082] In various embodiments of the invention, such as those described above, one or more sensors may be positioned to measure gas data within an interior portion of one of the nasal cannula's conduits, or to measure gas data adjacent an exterior portion of the cannula. In such embodiments, one or more sensors may be, for example, positioned adjacent an interior or exterior surface of the cannula. In certain embodiments of the invention, one or more of the cannula's sensors is adapted to monitor one or more of the following types of data within the cannula's conduits, or

adjacent the cannula's exterior surface (e.g., adjacent a side portion, or distal end of, one of the cannula's nasal inserts): (1) gas pressure; (2) gas flow rate; (3) carbon dioxide content; (4) temperature; (5) moisture level; and/or (6) oxygen content.

[0083] Absolute vs. Relative Pressure Measurements

[0084] In various embodiments of the invention, the cannula may be configured for sensing absolute pressure within, or adjacent, a particular portion of the cannula. Similarly, in particular embodiments, the cannula may be configured to measure the difference between the pressure at two different locations within the cannula. This may be done, for example, by providing two separate sensors (e.g., that are positioned in different locations within one of the cannula's conduits), or by providing two physically distinct gas intake conduits, each of which is adapted for routing gas from a different location within the cannula. For example, in various embodiments of the invention shown in Figure 1, the first inlet **152** may be connected to a first intake conduit that is adapted for routing gas to a first sensor, and the second inlet **154** may be connected to a physically separate second intake conduit that is adapted for routing gas to a second pressure sensor. Information from the first and second sensors may then be used to calculate the difference in pressure between the first and second inlets **152, 154**. Alternatively, a differential pressure sensor may be used.

[0085] Suitable Sensors

[0086] Suitable sensors for use with various embodiments of the invention include electronic and optical sensors. For example, suitable sensors may include: (1) Disposable MEM Piezoelectric sensors (e.g., from Silex Microsensors); (2) light-

based sensors such as a McCaul O₂ sensor - see U.S. Patent 6,150,661 to McCaul; and

(3) Micro-pressure sensors, such as those currently available from Honeywell.

[0087] Non-Sealing Feature

[0088] As shown in Figure 4, in various embodiments of the invention, one or more of the nasal cannula's nasal inserts **425, 430** defines one or more recesses **423** (e.g., grooves, semicircular recesses, or other indentations or conduits) that extend along a length of the nasal insert's exterior surface. As may be understood from this figure, in various embodiments of the invention, at least one of these recesses **423** is an elongate groove that extends from adjacent a distal surface of the nasal insert **325, 330, 425, 430** and past the midpoint between: (1) the nasal insert's distal surface and (2) the portion of the nasal insert **425, 430** that is immediately adjacent the nasal cannula's base portion **305, 405**. As may also be understood from this figure, in various embodiments of the invention, each groove **423** extends substantially parallel to the central axis of its respective nasal insert **425, 430**.

[0089] In particular embodiments of the invention, such as the embodiment shown in Figure 4, at least one of the nasal cannula's nasal inserts **425, 430** is configured so that when the nasal inserts **425, 430** are operatively positioned within a user's nares, the nasal inserts do not form an airtight seal with the user's nares. This may be due, for example, to the ability of air to flow adjacent the user's nare through recesses **423** in the nasal inserts **425, 430** when the user is wearing the nasal cannula.

[0090] Figures 5-8 depict additional embodiments of the invention that are configured so that when the cannula's nasal inserts are operatively positioned adjacent (e.g., partially within) the user's nares, the nasal inserts do not form a seal with the user's nares. For example, in the embodiment shown in Figure 5, at least one (and

preferably both) of the cannula's nasal inserts **525**, **530** comprise an inlet **555** (which may, for example, be substantially tubular), and one or more flange portions **560**, **561** that are adapted to maintain a physical separation between an exterior side surface of the inlet **555** and a user's nare when the nasal insert **525**, **530** is inserted into the user's nare.

[0091] For example, in the embodiment of the invention shown in Figure 5, each of the cannula's nasal inserts **525**, **530** includes a substantially tubular inlet **555** and a pair of co-facing, elongated flanges **560**, **561** that each have a substantially C-shaped cross section. In this embodiment, these C-shaped flanges **560**, **561** cooperate with a portion of the exterior of the inlet **555** to form a substantially U-shaped channel (which is one example of a "nasal lumen") through which ambient air may flow to and/or from a user's nasal passages when the cannula **500** is operatively in place within the user's nares. In this embodiment, when the nasal inserts **525**, **530** are properly in place within the user's nares, respiratory gas is free to flow into the user's nose through the inlet **555**, and ambient air is free to flow into and out of the user's nose through a passage defined by: (1) the flanges **560**, **561**; (2) the exterior side surface of the inlet **555** that extends between the flanges **560**, **561**; and (3) an interior portion of the user's nose. In various embodiments, air may flow to and/or from a user's nose through this passage when the cannula **500** is operatively in place within the user's nares. A pathway (e.g., a semicircular pathway) may be provided adjacent the interior end of this U-shaped channel, which may act as a passageway for gas exhaled and inhaled through the U-shaped channel.

[0092] The general embodiment shown in Figure 5 may have many different structural configurations. For example, as shown in Figure 6, which depicts a cross section of a nasal insert according to a particular embodiment of the invention, the

respiratory gas inlets of the cannula's nasal inserts **655** may be in the form of a tube having an irregular cross section (e.g., a substantially pie-piece-shaped cross section) rather than a circular cross section. Alternatively, as may be understood from Figure 7, the respiratory gas inlets of the cannula's nasal inserts **755** may be in the form of a tube having a substantially half-circular cross section rather than a circular cross section.

[0093] Similarly, as may be understood from Figures 6 and 7, the shape and size of the cannula's flanges may vary from embodiment to embodiment. For example, in the embodiment shown in Figure 6, each of the flanges **660**, **661** has a relatively short, substantially C-shaped cross section and the distal ends of flanges **660**, **661** are spaced apart from each other to form a gap. As shown in Figure 7, in other embodiments, each of the flanges **760**, **761** may have a relatively long, substantially C-shaped cross section and the distal ends of the flanges **760**, **761** may be positioned immediately adjacent each other.

[0094] As may be understood from Figure 7, in various embodiments of the invention, a separation **763** (e.g., a slit, such as an angular slit) is provided between the flanges **760**, **761**. This may allow the flanges **760**, **761** to move relative to each other and to thereby conform to the nare in which the nasal insert is inserted. In other embodiments, the cross section of the nasal inserts is substantially as that shown in Figure 7, except that no separation **763** is provided within the semi-circular flange portion. Accordingly, in this embodiment of the invention, a substantially semi-circular portion of the exterior of the air inlet cooperates with a substantially semi-circular portion of the flange portion to form an exterior having a contiguous, substantially circular cross section. One such embodiment is shown in Figures 8A – 8C.

[0095] As may be understood from Figures 8A – 8C, in this embodiment, when the cannula **800** is in use, respiratory gas may flow into the user's nose through passageways **881** (e.g., a portion of which may be defined by a corresponding respiratory gas inlet **855**) that extend through each of the cannula's nasal inserts **825**, **830**. A pathway **885** of substantially semi-circular cross section extends between the distal end of each nasal insert **825**, **830** to a substantially semicircular outlet **865** defined within the cannula's base **805**. In various embodiments, when the cannula **800** is in use, the user may inhale and exhale gas through this pathway **885**.

[0096] In certain embodiments, as discussed above, a conduit **850** is provided in each of the cannula's nasal inserts **825**, **830** (see Figure 8C). Each of these conduits **850** may be adapted to: (1) receive gas from the interior of a corresponding pathway **885** and/or from adjacent the exterior of one of the cannula's nasal inserts **825**, **830**, and (2) guide the gas out of a corresponding outlet **835**, **840** in the cannula **800**. As discussed above, one or more sensors may be disposed within, or adjacent, the conduit **850** and used to assess one or more attributes of gas flowing through or adjacent the conduit **850**.

[0097] It should be understood that the embodiments of the invention shown in Figures 4 – 8 and related embodiments may have utility with or without the use of sensors or sensor conduits. It should also be understood that the various nasal inserts may be configured to be disposed in any appropriate orientation within the user's nares when the cannula is operably positioned within the user's nares. For example, in one embodiment of the invention, the cannula may be positioned so that the cannula's nasal lumen is immediately adjacent, or so that it faces anterior-laterally away from, the user's nasal spine.

[0098] Turning to yet another embodiment of the invention, as shown in Figure 9, the cannula **900** and corresponding sensor may be adapted so that a tube inlet **970**, **972** for at least one sensor (or the sensor itself) is maintained adjacent, and spaced a pre-determined distance apart from, the distal end of a respective nasal insert **925**, **930**. In this embodiment, the sensor (or sensor intake inlet) may be spaced apart from the rest of the nasal cannula **900** adjacent one of the nasal cannula's outlet openings.

[0099] As may be understood from Figure 10, in various embodiments, the first and second nozzles **1026**, **1031** of the nasal cannula are configured to remain outside of the user's nares while the cannula is in use. For example, the nozzles may be of a length such that, when the cannula is in use, the distal ends of the nozzles **1026**, **1031** lie adjacent, but outside, the user's nares. By preventing insertion of the nozzles **1026**, **1031** into the nares, sealing of the nares can be avoided. As may be understood from Figure 13, in various embodiments, when the nasal cannula is in an operative position adjacent the user's nares, an outlet portion (and distal end) of each nozzle **1326**, **1331** is spaced apart from, and substantially in-line (e.g., substantially co-axial) with, a corresponding one of the patient's nares. In various embodiments, when the nasal cannula is operatively in use, the outlet of each nozzle is spaced apart from the patient's nares and each nozzle is positioned to direct a focused flow of gas into a particular respective one of the user's nares.

[00100] As may be understood from Figure 11, in particular embodiments, a stop **1190** may extend outwardly from the base portion **1105** of the nasal cannula. In some embodiments, the stop **1190** lies in between the first and second nozzles **1126**, **1131** and defines a central axis that runs substantially parallel to the respective central axes of the nozzles **1126**, **1131**. The stop **1190**, in some embodiments, may extend outwardly from the nasal cannula's base portion **1105** a length greater than that of the

nozzles **1126, 1131**. In this manner, the stop **1190** prevents the nozzles **1126, 1131** from being inserted into the user's nares when the nasal cannula **1100** is in use.

[00101] For example, the stop **1190** may be positioned so that when the nasal cannula **1100** is in use, the stop is designed to engage the columella of the user's nose and thereby prevent the nozzles **1126, 1131** from being inserted into the user's nares. In various embodiments, the first and second nozzles **1126, 1131** are positioned on either side of the stop **1190** so that when the nasal cannula **1100** is operatively in use, the each nozzle **1126, 1131** will be spaced apart from a respective particular one of the patient's nares and will be positioned to direct a focused flow of gas into that particular nare by, for example, being positioned so that the outlet (and distal end) of each nozzle (first outlet **1183** and second outlet **1184**) is substantially in-line (e.g., substantially co-axial) with, a corresponding one of the patient's nares.

[00102] As may be understood from Figure 12, in various embodiments, the nasal cannula **1200** may include only a single nozzle **1227**. The nozzle **1227**, in various embodiments, has an oblong or substantially elliptical cross-section. In these embodiments, the major axis of the ellipse runs substantially parallel to the central axis of the base portion **1205** of the nasal cannula. In one embodiment, the nozzle **1227** is wide enough to allow air to flow into both of a user's nares when the nasal cannula is in use. For example, in various embodiments, the width of the nozzle **1227** (e.g., a length defined by the major axis of the nozzle's elliptical cross section) may be approximately equal to (or greater than) the total width of the user's nares.

[00103] As may be understood from Figure 14, when the nasal cannula **1400** is operatively in use, a first lateral side **1430** of the nozzle outlet **1429** is spaced apart from, and adjacent, a user's first nare, and a second lateral side **1430** of the nozzle **1429** is spaced apart from, and adjacent, the user's second nare. In this and other

configurations, the nozzle **1422** is configured to direct a focused flow of gas simultaneously into each of the user's nares. In various embodiments, when the nozzle is of a width approximately equal to (or greater than) the total width of the user's nares, and other widths, the nozzle **1227** is sufficiently wide to prevent the nozzle **1227** from being inserted into a user's nare, thus preventing sealing of the nasal cannula with the nare.

[00104] In various other embodiments, the cannula's single nozzle may have a different cross-section that is not oblong or elliptical. For example, the nozzle may have a substantially circular cross-section, with a diameter that is wide enough to allow air to flow into both of a user's nares when the cannula is in use, while simultaneously being wide enough to prevent insertion into a single nare. In various other embodiments, the nasal cannula may have more than one nozzle, each having a substantially oblong cross section and a width that prevents insertion into each of a user's nares.

[00105] In various embodiments, one or more of the cannula's elongate extensions has a diameter that is adapted to prevent sealing with the user's nares. For example, the elongate extension(s) may have a diameter that is substantially narrower than a user's nares, so that sealing is avoided. In other embodiments, the elongate extension(s) may include features such as grooves or recesses, as described above, to prevent sealing when inserted into a user's nare(s).

[00106] Exemplary Use Of The Cannula

[00107] To use a cannula according to a particular embodiment of the invention, a physician or technician may have a patient use the cannula for a brief period of time, while the physician or technician monitors information received from the cannula's

various sensors, or the information may be recorded for later analysis. The physician or technician may then use this information to adjust the structure or operation of the cannula until the cannula's sensors indicate that the patient's upper airway environment satisfies certain conditions.

[00108] Similarly, in various embodiments, the cannula's sensors may be used to monitor conditions within the patient's upper airway over time. In a particular embodiment, the cannula's sensors may be connected to a control system that will automatically alter or modify the flow of therapeutic gas into the cannula if information from the sensor indicates undesirable conditions within the patient's upper airway. In further embodiments of the invention, the sensor is connected to a control system that issues an alarm if information from the cannula's sensors indicate undesirable conditions within the patient's airway.

[00109] Figures 13 and 14 depict various embodiments of nasal cannulas being used on a patient. As may be understood from Figure 13, for example, a nasal cannula is used on a young or small infant for high flow therapy. For example, a nasal cannula similar to that shown in Figure 10 can be used. In various embodiments, first and second elongate extensions **1370**, **1372** are inserted into the patient's nares, while corresponding first and second nozzles **1326**, **1331** remain adjacent and external to the patient's nares. As may be appreciated, when the nasal cannula is in use, air flows into the patient's nares via the nozzles. Figure 14 depicts one embodiment of a nasal cannula in use on a patient. In one embodiment, a nasal cannula such as that shown in Figure 12 can be used. As may be understood from Figure 14, a nasal cannula having a single nozzle **1427** can be used, in which the nozzle is sized and shaped (e.g., is elliptical and/or wider than a patient's nare) to prevent insertion into the patient's nares. In various other embodiments, nasal

cannula having nasal inserts, as described throughout, can be used. In these embodiments, the nasal inserts are inserted into the user's nares while the cannula is in use. Nasal cannula according to embodiments of the invention can be used on a variety of patients.

[00110] High Flow Therapy Device

[00111] Now referring to Figures 15 – 17, a high flow therapy device **2000** is shown. High flow therapy device **2000** is configured for use with a non-sealing respiratory interface, such as cannula **100**, for example, to deliver gas to a patient. In various embodiments, high flow therapy device **2000** is able to heat, humidify, and/or oxygenate a gas prior to delivering the gas to a patient. Additionally, embodiments of high flow therapy device **2000** are able to control and/or adjust the temperature of the gas, the humidity of the gas, the amount of oxygen in the gas, the flow rate of the gas and/or the volume of the gas delivered to the patient.

[00112] High flow therapy device **2000** is shown in Figure 15 including a housing **2010**, a humidity chamber **2020** (e.g., vapor generator), a user interface **2030**, a gas inlet port **2040** and a gas outlet port **2050**. A microprocessor **2060**, an air inlet port **2070**, a blower **2080**, an oxygen inlet **2090** and a proportional valve **2100** are illustrated in Figure 16. A non-sealing respiratory interface (such as a nasal cannula illustrated in Figures 1-14 (e.g., **100** or **1200** and hereinafter referred to as **100**), is configured to mechanically cooperate with gas outlet port **2050** to supply a patient with gas.

[00113] A heating element **2110** is shown schematically in Figure 17 (and is hidden from view by humidity chamber **2020** in Figure 15) is in electrical communication with microprocessor **2060** (which is included on printed circuit board

("PCB")), via wire **2112**, for instance, and is capable of heating a liquid (e.g., water) within humidity chamber **2020** to create a gas. Non-sealing respiratory interface **100** is configured to delivery this gas to a patient. Further, a sensor **2120** or transducer (shown in Figure 20) is disposed in electrical communication with microprocessor **2060** and is configured to measure pressure in the upper airway UA (including both the nasal cavity and the oral cavity) of a patient. In an embodiment, a conduit **2130** extends between the upper airway of the patient and sensor **2120** (Figure 19, sensor **2120** is not explicitly shown in Figure 19, but may be disposed adjacent microprocessor **2060**). In another embodiment, sensor **2120** is disposed at least partially within the upper airway of the patient with a wire **2122** relaying signals to microprocessor **2060** (Figures 18 and 20).

[00114] In use, a liquid (e.g., water) is inserted into humidity chamber **2020** through a chamber port **2022**, for instance. Heating element **2110** heats the liquid to create a vapor or gas. This vapor heats and humidifies the gas entering humidity chamber **2020** through gas inlet port **2040**. The heated and humidified vapor flows through gas outlet port **2050** and through non-sealing respiratory interface **100**.

[00115] In a disclosed embodiment, sensor **2120** collects data for the measurement of the patient's respiration rate, tidal volume and minute volume. Further, based on measurements taken by sensor **2120** and relayed to microprocessor **2060**, microprocessor **2060** is able to adjust the temperature of the gas, the humidity of the gas, the amount of oxygen of the gas, flow rate of the gas and/or the volume of the gas delivered to the patient. For example, if the pressure at the patient's upper airway is measured and determined to be too low (e.g., by a pre-programmed algorithm embedded on microprocessor **2060** or from a setting inputted by an operator),

microprocessor **2060** may, for example, adjust the speed of blower **2080** and/or oxygen proportional valve **2100** so that sufficient pressure levels are maintained.

[00116] Additionally, sensor **2120** may be used to monitor respiratory rates, and microprocessor **2060** may signal alarms if the respiratory rate exceeds or falls below a range determined by either microprocessor **2060** or set by an operator. For example, a high respiratory rate alarm may alert the operator and may indicate that the patient requires a higher flow rate and/or higher oxygen flow.

[00117] With reference to Figure 17, a pair of thermocouples **2200** and **2202** are illustrated, which detect the temperature entering and leaving a circuit **2210** disposed between respiratory interface **100** and gas outlet port **2050**. Further, a second heating element **2114** (or heater) (e.g., a heated wire) may be disposed adjacent air outlet port **2050** to further heat the gas. It is also envisioned that second heating element **2114** is disposed within circuit **2210**. Thermocouples **2200** and **2202** are in communication with microprocessor **2060** and may be used to adjust the temperature of heating element **2110** and second heating element **2114**. A feedback loop may be used to control the temperature of the delivered gas, as well as to control its humidity and to minimized rainout. Figure 16 illustrates an embodiment of circuit **2210** including conduit **2130** co-axially disposed therein, in accordance with an embodiment of the present disclosure.

[00118] Relating to the embodiment illustrated in Figure 16, blower **2080** is used to draw in ambient air from air inlet port **2070** and force it through an air flow tube **2140**, through gas inlet port **2040**, through humidity chamber **2020** and through gas outlet port **2050** towards non-sealing respiratory interface **100**. Blower **2080** is configured to provide a patient (e.g., an adult patient) with a gas flow rate of up to about 60 liters per minute. In a particular embodiment, it is envisioned that blower

2080 is configured to provide a patient with a gas flow rate of up to about 40 liters per minute. Additionally, an air intake filter **2072** (shown schematically in Figure 17) may be provided adjacent air inlet port **2070** to filter the ambient air being delivered to the patient. It is envisioned that air intake filter **2072** is configured to reduce the amount of particulates (including dust, pollen, fungi (including yeast, mold, spores, etc.) bacteria, viruses, allergenic material and/or pathogens) received by blower **2080**. Additionally, the use of blower **2080** may obviate the need for utilization of compressed air, for instance. It is also envisioned that a pressure sensor is disposed adjacent air intake filter **2072** (shown schematically in Figure 17), which may be capable of determining when air intake filter **2072** should be replaced (e.g., it is dirty, it is allowing negative pressure, etc).

[00119] With continued reference to Figure 16, oxygen inlet **2090** and is configured to connect to an external source of oxygen (or other gas) (not explicitly shown) to allow oxygen to pass through high flow therapy device **2000** and mix with ambient air, for instance. Proportional valve **2100**, being in electrical communication with microprocessor **2060**, is disposed adjacent oxygen inlet **2090** and is configured to adjust the amount of oxygen that flows from oxygen inlet **2090** through an oxygen flow tube **2150**. As shown in Figures 16 and 17, oxygen flowing through oxygen flow tube **2150** mixes with ambient air (or filtered air) flowing through air flow tube **2140** in a mixing area **2155** prior to entering humidity chamber **2020**.

[00120] In a disclosed embodiment, sensor **2120** measures both inspiration pressure and expiration pressure of the patient. In the embodiment illustrated in Figures 18 and 19, conduit **2130** delivers the pressure measurements to sensor **2120** (not explicitly shown in Figures 18 and 19), which may be disposed adjacent microprocessor **2060**. In the embodiment illustrated in Figure 20, sensor **2120** is

position adjacent the patient's upper airway and includes wire **2122** to transmit the readings to microprocessor **2060**.

[00121] In various instances, clinicians do not desire ambient air to enter a patient's upper airway. To determine if ambient air is entering a patient's upper airway (air entrainment), the inspiration and expiration pressure readings from within (or adjacent) the upper airway may be compared ambient air pressure. That is, a patient may be inhaling gas at a faster rate than the rate of gas that high flow therapy device **2000** is delivering to the patient. In such a circumstance (since respiratory interface **100** is non-sealing), in addition to breathing in the supplied gas, the patient also inhales ambient air. Based on this information, microprocessor **2060** of high flow therapy device **2000** is able to adjust various flow parameters, such as increasing the flow rate, to minimize or eliminate the entrainment of ambient air.

[00122] Figure 21 illustrates an example of a screen shot, which may be displayed on a portion of user interface **2030**. The crest of the sine-like wave represents expiration pressure and the valley represents inspiration pressure. In this situation, ambient air entrainment into the patient's upper airway is occurring as evidenced by the valley of the sine wave dipping below the zero-pressure line. Microprocessor **2060** may be configured to automatically adjust an aspect (e.g., increasing the flow rate) of the gas being supplied to the patient by high flow therapy device **2000** to overcome the entrainment of ambient air. Further, microprocessor **2060** may convey the pressure readings to the operator who may then input settings to adjust the flow rate to minimize entrainment of ambient air or to maintain a level of pressure above the ambient air pressure. Further, lowering the flow rates during expiration may also minimize oxygen flow through high flow therapy device **2000**. Such lowering of a flow rate may also minimize entry of oxygen into a closed environment, such as the

patient room or the interior of an ambulance, where high levels of oxygen might be hazardous.

[00123] In a disclosed embodiment, conduit 2130 may be used as a gas analyzer which may be configured to take various measurements (e.g., percent of oxygen, percentage of carbon dioxide, pressure, temperature, etc.) of air in or adjacent a patient's upper airway.

[00124] In another embodiment (not explicitly illustrated), a gas port may be disposed adjacent housing 2010 to communicate with exterior of housing 2010. It is envisioned that the gas port is configured to allow the use of external devices to measure various gas properties (e.g., percent oxygen and pressure). Additionally, the gas port may be used for external verification of gas values. Further, a communications port 2300, shown in Figure 16, may be included to facilitate connection with an external device, such as a computer, for additional analysis, for instance. Further, communications port 2300 enables connection with another device, enabling data to be monitored distantly, recorded and/or reprogrammed, for example.

[00125] A directional valve 2160 and/or a sample pump 2170 (schematically shown in Figure 17) may also be included to facilitate sampling the gas for analysis. More specifically, in a particular embodiment, sample pump 2170 is capable of moving a quantity of gas towards the gas analyzer. As shown schematically in Figure 17, the gas sample can be taken from a patient's upper airway via conduit 2130 or from mixing area 2155 via a sample line 2180 and a sample port 2182 (Figure 16). Directional valve 2160 may be controlled by microprocessor 2060 to direct a gas sample from either location (or a different location such as after the gas is heated). The gas analyzer can compare measurements of the gas sample(s) with predetermined measurements to ensure high flow therapy device 2000 is working optimally. It is

further envisioned that sample pump **2170** may be configured to pump a gas or liquid towards the patient to provide the patient with an additional gas, such as an anesthetic, for instance and/or to clean or purge conduit **2130**.

[00126] The present disclosure also relates to methods of supplying a patient with gas. The method includes providing high flow therapy device **2000**, as described above, for example, heating the gas, and delivering the gas to the patient. In this embodiment, high flow therapy device **2000** includes microprocessor **2060**, heating element **2110** disposed in electrical communication with microprocessor **2060**, non-sealing respiratory interface **100** configured to deliver gas to the patient and sensor **2120** disposed in electrical communication with microprocessor **2060** and configured to measure pressure in the upper airway of the patient. The method of this embodiment may be used, for instance, to provide a patient with respiratory assistance. Blower **2080** may also be included in high flow therapy device **2000** of this method. Blower **2080** enables ambient air to enter high flow therapy device **2000** (e.g., through filter **2072**) and be supplied to the patient. In such an embodiment, high flow therapy device is portable, as it does not need an external source of compressed air, for example.

[00127] Another method of the present disclosure relates to minimizing respiratory infections of a patient. In an embodiment of this method, high flow therapy device **2000** includes heating element **2110** and non-sealing respiratory interface **100**. Here, a patient may be provided with heated and/or humidified air (e.g., at varying flow rates) to help minimize respiratory infections of the patient. Further, such a method may be used in connection with certain filters **2072** to help prevent patients from obtaining various conditions associated with inhaling contaminated air, such as in a hospital. Additionally, providing appropriately warmed and humidified respiratory

gases optimizes the motion of the cilia that line the respiratory passages from the anterior third of the nose to the beginning of the respiratory bronchioles, further minimizing risk of infection. Further, supplemental oxygen may add to this effect. Microprocessor **2060** in connection with sensor **2120** may also be included with high flow therapy device **2000** of this method for measuring and controlling various aspects of the gas being delivered to the patient, for instance, as described above.

[00128] A further method of the present disclosure relates to another way of supplying a patient with gas. The present method includes providing high flow therapy device **2000** including heating element **2110**, non-sealing respiratory interface **100**, blower **2080**, air inlet port **2070** configured to enable ambient air to flow towards blower **2080** and filter **2070** disposed in mechanical cooperation with air inlet port **2070** and configured to remove pathogens from the ambient air. High flow therapy device **2000** of this method may also include microprocessor **2060** and sensor **2120**.

[00129] Another method of the present disclosure includes the use of high flow therapy device **2000** to treat headaches, upper airway resistance syndrome, obstructive sleep apnea, hypopnea and/or snoring. High flow therapy device **2000** may be set to provide sufficient airway pressure to minimize the collapse of the upper airway during inspiration, especially while the use is asleep. HFT may be more acceptable to children and other who may not tolerate traditional CPAP therapy which requires a sealing interface. Early treatment with HFT may prevent the progression of mild upper airway resistance syndrome to more advanced conditions such as sleep apnea and its associated morbidity.

[00130] Another method of the present disclosure is the treatment of headaches using HFT. In an embodiment of treating/preventing headaches, gas may be delivered to patient at a temperature of between about 32°C and about 40°C (temperature in the

higher end of this range may provide a more rapid response) and having at least about 27 milligrams of water vapor per liter. More specifically, it is envisioned that a gas having a water vapor content of between about 33 mg/liter and about 44 mg/liter may be used. It is envisioned that the gas being delivered to the patient includes moisture content that is similar to that of a typical exhaled breath. In an embodiment, the flow rates of this heated and humidified air are sufficient to prevent/minimize entrainment of ambient air into the respired gas during inspiration, as discussed above. The inclusion of an increased percentage of oxygen may also be helpful. Further, the gas may be delivered to the patient using non-sealing respiratory interface **100**.

[00131] High flow therapy device **2000** used in these methods includes heating element **2110** and non-sealing respiratory interface **100**. Microprocessor **2060** and sensor **2120** may also be included in high flow therapy device **2000** of this method. The inclusion of blower **2080**, in accordance with a disclosed embodiment, enables high flow therapy device **2000** to be portable, as it does not need to be connected to an external source of compressed air or oxygen. Thus, high flow therapy device **2000** of this method is able to be used, relatively easily, in a person's home, a doctor's office, an ambulance, etc.

[00132] The present disclosure also relates to a method of delivering respiratory gas to a patient and includes monitoring the respiratory phase of the patient. Monitoring of a patient's respiratory phase is enabled by taking measurements of pressure in a patient's upper airway. Additionally, respiratory phase may be determined by pressure with circuit **2210** or by monitoring activity of the phrenic nerve. Real-time pressure measurements (see sine-like wave in Figure 21, for example) enable real-time supplying of gas at different pressures to be delivered to the patient, or variable pressure delivery. For example, gas at a higher pressure may

be delivered to the patient during inspiration and gas at a lower pressure may be delivered to the patient during expiration. This example may be useful when a patient is weak and has difficulty exhaling against an incoming gas at a high pressure. It is further envisioned that the pressure level of the gas being delivered to a patient is gradually increased (e.g., over several minutes) to improve patient comfort, for instance.

[00133] With reference to Figures 22-24, mouthpiece **3000** is illustrated in accordance with an embodiment of the present disclosure. As briefly described above, mouthpiece **3000** is an example of a respiratory interface of the present disclosure. Mouthpiece **3000** (illustrated resembling a pacifier) may be used to detect upper airway pressure of a patient.

[00134] A first mouthpiece port **3010** may be used to measure pressure inside mouthpiece **3000** through open end 3012 of first port. First mouthpiece port **3010** may include an open-ended tube that communicates the pressure with mouthpiece **3000** to sensor **2120** (not explicitly shown in Figures 22-24) via first port conduit **2130a**. Sensor **2120** may also be positioned within mouthpiece **3000**. It is envisioned that mouthpiece **3000** is at least partially filled with a gas or liquid, e.g., water.

[00135] The pressure within mouthpiece **3000** may help evaluate, record or otherwise use the pressure data for determining the strength of sucking or feeding, for instance. The timing of the sucking motion and the differential pressures in the mouth may also be measured. The sucking pressure may be used to help determine the strength of the sucking and may be used to evaluate the health of an infant, for instance. The measurement of oral-pharyngeal pressure may also give data for setting or adjusting respiratory support therapy for the patient. It is envisioned that a relatively short first mouthpiece port **3010** may be used so that a bulb **3030** of

mouthpiece **3000** acts as a pressure balloon. It is also envisioned that a relatively long first mouthpiece port **3010** having rigidity may be used to help prevent closure of the tube from pressure from alveolar ridges or from teeth, for example.

[00136] A second mouthpiece port **3020** is configured to enter a patient's mouth or oral cavity when mouthpiece **3000** is in use and is configured to measure pressure within the oral cavity (upper airway pressure) through an open end **3022** of second mouthpiece port **3020**. Pressure from within the upper airway (e.g., measured adjacent the pharynx) may be transmitted to sensor **2120** via second port conduit **2130b** or sensor **2120** may be positioned adjacent mouthpiece **3000**. That is, the pressure communicated from within the upper airway to the patient's mouth is the pressure being measured. It is envisioned that second mouthpiece port **3020** extends beyond a tip of bulb **3030** to facilitate the acquisition of an accurate upper airway pressure measurement.

[00137] Referring to Figure 23, a balloon **3040** is shown adjacent a distal end **3024** of second port **3020**. Here, it is envisioned that a lumen of conduit **2130b** is in fluid communication with the internal area of balloon **3040**. Further, any forces against a wall of balloon **3040** are transmitted through the lumen towards sensor **2120** or transducer for control, observation or analysis.

[00138] The pressure within the oral cavity may vary during the phases of sucking and swallowing. High flow therapy device **2000** using mouthpiece **3000** enables concurrent measurement of sucking pressure within mouthpiece **3000** and the pressure outside mouthpiece **3000**. This data may help determine treatment characteristics for respiratory support for infants, children or adults, e.g., unconscious adults.

[00139] In an embodiment of the present disclosure, high flow therapy device or system **2000** includes microprocessor **2060**, heating element **2110**, humidity chamber

2020, conduit 2130, blower 2080 and a feedback system. The heating element 2110 is disposed in electrical communication with the microprocessor 2060 and is capable of heating a liquid to create a gas. The humidity chamber 2020 is disposed in mechanical cooperation with the heating element 2110. The conduit 2130 is configured to direct the gas towards a patient. The blower 2080 is disposed in electrical communication with the microprocessor 2060 and is capable of advancing the gas at least partially through the conduit 2130. The feedback system is configured to control a volume of gas being directed towards the patient.

[00140] In an embodiment, it is envisioned that at least one gas flow sensor 2120 is disposed in electrical communication with the microprocessor 2060 and is configured to detect at least one flow characteristic of the gas. It is envisioned that high flow therapy system 2000 includes at least one compressed gas entry port 2090. Further, a pulse oximeter (see FIG. 17A), as discussed below, may be incorporated into high flow therapy system of the present disclosure.

[00141] The present disclosure also relates to a high flow therapy system 2000 including a microprocessor 2060, a heating element 2110, a humidity chamber 2020, a conduit 2130, at least one proportional valve 2132 (see Figs. 32A and 32B) and a feedback system. The heating element 2110 is disposed in electrical communication with the microprocessor 2060 and is capable of heating a liquid to create a gas. The humidity chamber 2020 is disposed in mechanical cooperation with the heating element 2110. The conduit 2130 is configured to direct the gas towards a patient. The at least one proportion valve 2132 is disposed in electrical communication with the microprocessor 2060 and is configured to help control the entry and passage of gas. The feedback system is configured for controlling a volume of gas directed towards the patient. It is noted that, while the blower 2080 is not necessarily part of

the other embodiments of the present disclosure, this embodiment specifically does not include a blower 2080.

[00142] It is envisioned that the high flow therapy system 2000 of this embodiment includes at least one gas flow sensor 2120 disposed in electrical communication with the microprocessor 2060 and is configured to detect at least one flow characteristic of the gas.

[00143] The present disclosure also relates to a method for delivering heated and humidified gas to a patient. The method includes the steps of providing a high flow therapy device, providing a non-sealing respiratory interface (e.g., 100), providing a sensor 2120, delivering gas from the high flow therapy device to a patient, and measuring the flow rate of the gas delivery to the patient. The high flow therapy device includes a heating element 2110 capable of heating a liquid to create a gas. The non-sealing respiratory interface is disposed in mechanical cooperation with the high flow therapy device and is configured to direct the gas towards a patient. The sensor is disposed in electrical communication with a microprocessor 2060 of the high flow therapy device and is configured to measure a flow rate of the gas delivered to the patient. An optional step of the method includes increasing (e.g., gradually increasing) the flow rate of the gas delivered to the patient.

[00144] With reference to Figures 25-28, a connector 4000 for use a system for delivery of respiratory gases (e.g., high flow therapy device 2000) is shown. Connector 4000 includes a gas lumen 4010 and a pressure conduit 4020. Gas lumen 4010 is configured to link a gas outlet 4110 of a therapy device 4100 (e.g., high flow therapy device 2000) with a gas inlet 4210 of a delivery conduit 4200. Pressure conduit 4020 is configured for engagement with at least one of a pressure port and a pressure sensor (collectively referred to as pressure port 4120 herein) of therapy

device 4100 and with at least one pressure conduit 4220 of delivery conduit 4200. It is envisioned that a seal 4122 (e.g., an O-ring seal) is disposed adjacent pressure port 4210 (see FIGS. 25 and 27).

[00145] In the embodiment illustrated in Fig. 26, connector 4000 also includes two temperature sensor (e.g., thermister or thermocouple) contacts 4030a, 4030b (shown in FIG. 28 on a lead wire) configured for engagement with temperature sensor contacts 4130a, 4130b of therapy device 4100 and with temperature sensors 4230a, 4230b of delivery conduit 4200. Figure 26 also illustrates an electrical contact 4040 disposed on connector 4000. Electrical contact 4040 is configured for engagement with an electrical contact 4140 of therapy device 4100 and with a heating element 4240 of delivery conduit 4200. It is envisioned that electrical contact 4040 is configured to signal microprocessor 2060 to provide power to a heat transfer plate 4610 (discussed below) and/or heating element 4240.

[00146] With specific reference to Fig. 27, a portion of pressure conduit 4020 of connector 4000 is coaxially disposed with gas lumen 4010 of connector. It is envisioned that pressure conduit 4020 is configured to convey gas, electricity and/or light between a patient and therapy device 4100.

[00147] It is therefore envisioned that various connections may be made with a single motion. That is, a gas connection, a pressure connection, at least one temperature sensor contact connection, and an electrical connection may be made by approximating connector 4000 (coupled to delivery conduit 4200) with therapy device 4100.

[00148] It is further envisioned that connector 4000 is configured to connect at least one optical fiber, electrical wire and/or pressure conduit from a delivery conduit 4200 with therapy device 4100 in a single motion. This may be helpful when sensing

temperature, pressure, flow, CO₂, O₂, Oxyhemoglobin saturation and other clinical measures from sensors operatively coupled to an airway interface or therapy device 4100.

[00149] Pulse oximetry, carbon dioxide and O₂ detection may thus be integrated into the HFT device (e.g., 4100) helping allow alarms to be incorporated based on data from at least one of a gas sensor, pulse oximetry, respiratory rate, tidal volume, pressure and from synthesis of clinical data. For instance, HFT device 4100 may include a pulse oximeter (schematically illustrated in FIG. 17A as part of printed circuit board box 2060). Pulse oximeter 2060 may be in the form of a microchip coupled with the printed circuit board and may include a probe 2062 and a wire 2064. In a disclosed embodiment (see FIG. 35), probe 2062 is connectable to a patient's ear lobe and wire 2064 connects probe 2062 with printed circuit board 2060 of HFT device 4100.

[00150] The HFT system may calculate cardiac output from data gathered from sensors. Data from sensors may be used in a feedback system to control at least one of FiO₂ and flow rate. The system may limit control to within pre-selected ranges. For example, FiO₂ could be set to be delivered in a range from about 21 percent to about 30 percent depending on pulse oximetry results, and an alarm could notify if the O₂ saturation from pulse oximetry fell below a set value for example, below 90 percent.

[00151] Figure 32A and 32B illustrate a schematic diagram of a further embodiment of an HFT device which allows for relatively low percentage gas mixtures, for example low FiO₂ when O₂ is mixed with air. In weaning a patient from O₂ therapy, it may be desirable to decrease a patient from a high percentage of FiO₂ to a low percentage of FiO₂, and in this case very small flows of O₂ may be

needed in a mixture with air. For example, to deliver an FiO_2 of 25 percent at 5 liters per minute, as may be used in HFT in neonates, about 4.75 liters of air would be mixed with .025 liters of O_2 . Conversely, to get a mixture of gases at higher ranges of O_2 , low amounts of air would be mixed with O_2 . The schematic illustrates how two proportional valves 2132 may be used to control flow over a wider range than would be effective with a single proportional valve. Also shown is how a single sensor may be configured to sense flow from two flow tubes (e.g., pneumotachs), in this instance, one for high and one for low volume flows.

[00152] HFT may be desirable for use in patients in locations where compressed or liquid O_2 is not readily or economically feasible. For patients who may benefit from oxygen therapy, an HFT device (e.g., 4100) may deliver gas from an oxygen concentrator. This gas may be mixed with room air. If 20 liters per minute room air is mixed with 6 liters per minute of O_2 from an oxygen concentrator delivering O_2 at 85% purity, the delivered gas mixture will have an O_2 concentration of about 36%. A higher concentration may be reached with the use of more than one oxygen concentrator.

[00153] The present disclosure also relates to a therapy system 4500 including delivery conduit (such as delivery conduit 4200 described herein), therapy device (such as therapy device 4100 described herein), and connector (such as connector 4000 described herein). Delivery conduit 4200 is configured to direct gas towards a patient interface. Therapy device 4100 is configured to supply gas to delivery conduit 4200. Connector 4000 is configured to operatively connect delivery conduit 4200 with therapy device 4100, e.g., in a single motion.

[00154] With reference to Figs. 29-29C, various embodiments of a humidity chamber 4600 for use with a therapy device (e.g., therapy device 4100) are shown.

With particular reference to Figs. 29 and 29A, humidity chamber 4600 includes heat transfer plate 4610 (e.g., made of aluminum) and a housing 4620 (e.g., made of thermoplastic). Housing 4620 includes a flange 4622 and a fixed barrier 4624. Flange 4622 is configured for engagement with a lip 4612 of heat transfer plate 4610. Fixed barrier 4624 extends along at least a portion of flange 4622 and is configured to shield an edge 4614 of heat transfer plate 4610.

[00155] As shown in Fig. 29B, an embodiment of humidity chamber 4600 includes an overhang 4626 extending from flange 4622/barrier 4624 and also includes a protrusion 4628 shown extending substantially vertically from flange 4622.

[00156] In the embodiment shown in Fig. 29C, humidity chamber 4600 also includes a plurality of ribs 4630 extending from a portion of housing 4620 and flange 4622. It is envisioned that a distance “d” between adjacent ribs 4630 is sufficiently small enough to prevent a user’s finger from contacting flange 4622. For example, distance “d” may be between about 0.5 cm and about 1.0 cm.

[00157] As can be appreciated, various features of Figs. 29-29C are helpful in protecting users from contacting a heated surface. Heat transfer plate 4610 is disposed in thermal communication with a heater plate (not explicitly shown in Figs. 29-29C) of therapy device 4100. Thus, heat transfer plate 4610 (e.g., edge 4614 of heat transfer plate 4610) may reach a temperature that exceeds safety standards for an exposed surface. In the present disclosure, flange 4622 is positionable adjacent lip 4612 of heat transfer plate 4610 to help prevent an exposed surface from exceeding an allowable amount. The inclusion of other features (e.g., fixed barrier 4624, overhang 4626, protrusion 4628, and plurality of ribs 4630) of the present disclosure may further help prevent a user from being able to contact a surface having a temperature that exceeds safety standards.

[00158] Additionally, humidity chamber 4600 may also include a bonding agent 4640 disposed between lip 4612 of heat transfer plate 4610 and flange 4622 of housing 4620. Bonding agent 4640 (e.g., made from Dymax Medical Class VI Approved UV Cure Acrylic adhesive, or Star*Tech Medical Class VI Approved UV Cure Acrylic Adhesive) may be configured and positioned to provide a substantially watertight seal between heat transfer plate 4610 and housing 4620.

[00159] An embodiment of the present disclosure includes a humidity chamber 6000 that may be opened and washed (e.g., in a dishwasher), as shown in Figs. 33A-33C. This allows for more economic use of an HFT device in the home. The upper housing 6010 is open and configured to mate with a seal 6020 (e.g., rubber or silicone) and a lid 6030. While various structure may be used to allow for a removable portion (e.g., a removable lid), the figures show the lid 6030 having one or more detachable hinges 6040a, 6040b on one surface which allow the lid 6030 to swing open to fill or refill the chamber. On the opposite surface a latch 6050 is included to help seal the lid 6030 closed. It is envisioned that the lid 6030 can be detached for washing.

[00160] With continued reference to Figs. 33A-33C, humidity chamber 6000 illustrated in this embodiment also includes a gas inlet 6060, a gas outlet (not explicitly shown in the illustrated embodiments), a condensation bar 6070, finger protection flanges 6080, an overhang 6090 and a depression 6100 in lid 6030. Condensation bar 6070 is configured to help keep condensation from running out in rear of chamber when lid 6030 is open for refilling. It is envisioned that the chamber is configured to allow refilling without removing the chamber from the HFT device and thus allows fluid to be poured therein rather than solely relying on refilling via an IV bag. As shown, front latch 6040b helps enable lid 6030 to open. Overhang 6090

is configured to help seat lid 6030 correctly and to hold seal 6020 in place.

Depression 6100 in lid 6030 is configured to act as a low point for the drippage of condensation.

[00161] Referring now to Figs. 30 and 31, a connector 5000 for use with a therapy device (e.g., therapy device 4200) is shown. Connector 5000 includes a conduit fitting 5100 and a cannula fitting 5200. Conduit fitting 5100 includes a gas lumen 5110 and a pressure lumen 5120. Gas lumen 5110 is configured to direct gas from therapy device 4200 towards a patient interface (e.g., non-sealing respiratory interface 100). Pressure lumen 5120 is configured to convey pressure from a patient interface 100 towards pressure port 4120 of therapy device 4100. Cannula fitting 5200 is configured for releasable engagement (e.g., coaxial engagement) with conduit fitting 5100 and includes at least one gas lumen 5210 and at least one pressure lumen 5220. The at least one gas lumen 5210 of conduit fitting 5200 is configured to direct gas from therapy device 4100 towards patient interface 100. The at least one pressure lumen 5220 is operatively engagable with pressure lumen 5120 and is configured to convey pressure from patient interface 100 towards pressure port 4120 of therapy device 4100.

[00162] In the illustrated embodiments, a distal portion 5202 of cannula fitting 5200 includes two gas lumens 5210a and 5210b, which are in gaseous communication with gas lumen 5210c of a proximal portion 5204 of cannula fitting 5200. The illustrated embodiments also illustrate distal portion 5202 of cannula fitting 5200 includes two pressure lumens 5220a, 5220b in gaseous communication with pressure lumen 5220c of proximal portion 5204 of cannula fitting 5200. In this embodiments, gas may be supplied to and/or pressure may be taken from each of a patient's nostrils.

[00163] With continued reference to Figs. 30 and 31, connector 5000 further includes at least one spoke 5300 (three spokes 5300a, 5300b and 5300c are shown) connecting a wall 5106 of conduit fitting 5100 and a wall 5122 of pressure lumen 5120 of conduit fitting 5100. Spoke 5300 is configured to allow axial movement (e.g., in the substantial directions of arrow "A" in Fig. 30) of pressure lumen 5120 of conduit fitting 5100 relative to wall 5106 of conduit fitting. Thus, a pressure seal may be created between pressure lumen 5120 of conduit fitting 5100 and at least one pressure lumen 5220 of cannula fitting 5200 prior to a gas seal being created between gas lumen 5110 of conduit fitting 5100 and at least one gas lumen 5210 of cannula fitting 5200. That is, at least one spoke 5300 facilitates a single-motion connection between conduit fitting 5100 and cannula fitting 5200, e.g., by allowing pressure lumens 5120, 5220 to axially move together, while attempting to operatively couple (e.g., create a gas seal) gas lumens 5110, 5210.

[00164] It should also be noted that while spokes 5300 are illustrated and described as being part of conduit fitting 5100, it is envisioned and within the scope of the present disclosure to include at least one spoke 5300 on cannula fitting 5200 in addition to or alternatively from providing at least one spoke 5300 on conduit fitting 5100.

[00165] An embodiment of the present disclosure also relates to a therapy device including a gas delivery conduit that allows for delivery of therapeutic gases which may be warmed and humidified and delivered to a subject. A second conduit allows pressure from the subject's airway to be communicated to a sensor within the therapy device. This second conduit may be a gas conduit and may also allow for sampling of gas from the subject's airway. Such an embodiment may be useful, for example, in determining the end expiratory CO₂ of the subject using the device.

[00166] In another embodiment, one or more pressure, temperature or other sensors may be placed in the subject's airway and may be used to provide data about the status of the subject receiving therapy and the subject's interaction with the therapy. Such sensors may be in electrical communication with a microprocessor 2060, and electric wires may be configured to follow or be within the delivery conduit. Data from sensors may also be transmitted optically. Optical fibers may transmit light which may be used to determine data about the subject's status and about the subject's interaction with the therapy. Optical fibers may be used in conjunction with certain sensors or in collaboration with electrical sensors. Further, optical fibers may be configured to follow or be disposed within the delivery conduit. The connector used in this embodiment may include contacts for a gas port for sensors, electrical contacts for sensors and/or optical connectors.

[00167] Running the HFT unit without water could deliver dry warm air to the user. One aspect of the present disclosure is the ability of the unit to give a signal which notifies the user that the unit has run low on water or is out of water to supply the needs to humidify the gas delivered. At least one of temperature data and power data of the heaters can be used to determine status of the water level in the humidity chamber 2020. Additional aspects of the present disclosure include the ability of the unit to signal a low water status, and to shut itself off or re-adjust flow and heater settings in response to low water. Another aspect of the present disclosure is the ability to trigger automatic refilling of the humidity chamber with water, by opening a valve controlling the inlet of an appropriate amount of water upon a signal from the microprocessor 2060.

[00168] After use, water or moisture may remain in the humidity chamber 2020 or conduit. This is a potential area for growth of microbes. Another aspect of the

present disclosure is a drying cycle, where the heater and blower are active, and run until the humidity chamber 2020 and the conduit are substantially dry. This helps prevent the growth of common microbes in the humidity chamber 2020 and the conduit. It is envisioned that monitoring at least one of temperature and current use by the unit helps control the drying cycle. That is, it is envisioned that microprocessor 2060 is able to detect changes in electrical current use and/or temperature data and can use this information to determine that the amount of water in the humidity chamber is inadequate for continued use. In response to an inadequate amount of water, microprocessor 2060 may trigger an auditory and/or visual signal, may trigger a mechanism (e.g., water supply) to add water to the chamber, and/or may adjust the delivered gas flow temperature and/or flow rate.

[00169] Figures 34A-34D illustrate a saddle 7000 where a portion of the conduit may be seated. In one configuration, the user places a portion of the conduit in a saddle 7000, or other connector. It is envisioned that when the conduit is positioned in the saddle 7000, a signal is sent to the unit to run the drying cycle until the humidity chamber 2020 and the conduit are dry and then to turn the unit off. It is also envisioned that the saddle 7000 is configured to help prevent the unit from being used by a patient during the drying cycle, which may operate at higher temperatures. In such an embodiment, it is envisioned that there are sensors 7100a, 7100b (e.g., electrical sensors, magnetic sensors, mechanical sensors, etc.) disposed on the saddle 7000 and the conduit that must be engaged with one another to enable the drying cycle to run.

[00170] Conclusion

[00171] Many modifications and other embodiments of the inventions set forth herein will come to mind to one skilled in the art to which these inventions pertain having the benefit of the teachings presented in the foregoing descriptions and the associated drawings. Therefore, it is to be understood that the inventions are not to be limited to the specific embodiments disclosed and that modifications and other embodiments are intended to be included within the scope of the appended claims. For example, although the embodiment shown in Figure 1 shows each nasal insert **125, 130** having a two inlets **152, 154**, in alternative embodiments of the invention, one or more of the nasal inserts **125, 130** may have more or less than two inlets (and/or more or less than two sensors). Further, sensors such as sensor **2120** may be situated or in communication with any area of the airway or with an artificial airway (such as that described in Provisional Application Serial No._____, filed on November 29, 2007; attorney docket no. 1573-11, express mail label no. EM 109 153 854 US), and is not limited to sensing the environment of the anterior nares. Although specific terms are employed herein, they are used in a generic and descriptive sense only and not for purposes of limitation.

What is claimed is:

1. A connector for use with a system for delivery of respiratory gases, the connector comprising:
 - a gas lumen configured to link a gas outlet of a therapy device with a gas inlet of a delivery conduit; and
 - a conduit configured for engagement with at least one of a pressure port and a sensor of the therapy device and with at least one conduit of the delivery conduit.
2. The connector of Claim 1, further including at least one temperature sensor contact configured for engagement with at least one temperature sensor contact of the therapy device and with at least one temperature sensor of the delivery conduit.
3. The connector of Claim 1, further including an electrical contact configured for engagement with an electrical contact of the therapy device and with a heating element of the delivery conduit.
4. The connector of Claim 2, further including an electrical contact configured for engagement with an electrical contact of the therapy device and with a heating element of the delivery conduit.
5. The connector of Claim 1, wherein at least a portion of the conduit is coaxially disposed within the gas lumen.
6. The connector of Claim 1, wherein the conduit is configured to convey at least one of pressure, gas, electricity and light.

7. A therapy system, comprising:
- a delivery conduit configured to direct gas towards a patient interface, the delivery conduit including:
 - a gas inlet; and
 - at least one pressure conduit;
 - a therapy device configured to supply gas to the delivery conduit, the therapy device, including:
 - a gas outlet; and
 - a pressure port;
 - a connector configured to operatively connect the delivery conduit with the therapy device, the connector including:
 - a gas lumen configured to link the gas outlet of the therapy device with the gas inlet of the delivery conduit; and
 - a pressure conduit configured for engagement with the pressure port of the therapy device and with the at least one pressure conduit of the delivery conduit.
8. The therapy system of Claim 7, further including at least one temperature sensor disposed at least partially within the delivery conduit, at least one temperature sensor contact disposed on the therapy device and a temperature sensor contact disposed on the connector, the temperature sensor contact of the connector configured for engagement with the at least one temperature sensor contact of the therapy device and with the at least one temperature sensor of the delivery conduit.

9. The therapy system of Claim 7, further including a heating element disposed within delivery conduit, an electrical contact disposed on the therapy device and an electrical contact disposed on the connector, the electrical contact disposed on the connector configured for engagement with the electrical contact of the therapy device and with the heating element of the delivery conduit.

10. The therapy system of Claim 7, wherein at least a portion of the pressure conduit of the connector is coaxially disposed within the gas lumen of the connector.

11. The connector of Claim 7, wherein the connector is configured to connect both the gas inlet of the delivery conduit with the gas outlet of the therapy device and the at least one pressure conduit of the delivery conduit with the pressure port of the therapy device in a single motion.

12. A connector for use with a therapy device, the connector comprising:
a conduit fitting including a gas lumen configured to direct gas from a therapy device towards a patient interface and a pressure lumen configured to convey pressure from a patient interface towards a pressure port of the therapy device; and

a cannula fitting configured for releasable engagement with the conduit fitting, the cannula fitting including at least one gas lumen and at least one pressure lumen, the at least one gas lumen being operatively engagable with the gas lumen of the conduit fitting and being configured to direct gas from the therapy device towards the patient interface, the at least one pressure lumen being operatively engagable with the pressure lumen of the conduit fitting and being configured to convey pressure from the patient interface towards the pressure port of the therapy device.

13. The connector of Claim 12, wherein a distal portion of the cannula fitting includes two gas lumens, wherein a proximal portion of the cannula fitting includes one gas lumen, and wherein the two gas lumens of the distal portion of the cannula fitting are in gaseous communication with the one gas lumen of the proximal portion of the cannula fitting.

14. The connector of Claim 12, wherein a distal portion of the cannula fitting includes two pressure lumens, wherein a proximal portion of the cannula fitting includes one pressure lumen, and wherein the two pressure lumens of the distal portion of the cannula fitting are in gaseous communication with the one pressure lumen of the proximal portion of the cannula fitting.

15. The connector of Claim 12, wherein at least a portion of the cannula fitting and at least a portion of the conduit fitting configured for coaxial engagement with one another.

16. The connector of Claim 12, further including at least one spoke connecting a wall of the conduit fitting and the pressure lumen of the conduit fitting, the at least one spoke configured to allow axial movement of the pressure lumen of the conduit fitting relative to the wall of the conduit fitting, thereby allowing a pressure seal to be created between the pressure lumen of the conduit fitting and the at least one pressure lumen of the cannula fitting prior to a gas seal being created between the gas lumen of the conduit fitting and the at least one gas lumen of the cannula fitting.

17. A humidity chamber for use with a therapy device, the humidity chamber comprising:
- a heat transfer plate; and
 - a housing including a flange and a fixed barrier, the flange configured for engagement with a lip of the heat transfer plate, the fixed barrier extending along at least a portion of the flange and configured to shield an edge of the heat transfer plate.
18. The humidity chamber of Claim 17, further including a plurality of ribs extending from at least one of a body of the housing and the flange.
19. The humidity chamber of Claim 17, further including a bonding agent disposed between the lip of the heat transfer plate and the flange of the housing, the bonding agent configured to provide a substantially watertight seal between the heat transfer plate and the housing.
20. The humidity chamber of Claim 17, wherein the housing includes a removable and resealable lid to facilitate cleaning.
21. A high flow therapy system, comprising:
- a microprocessor;
 - a heating element disposed in electrical communication with the microprocessor and capable of heating a liquid to create a gas;
 - a humidity chamber disposed in mechanical cooperation with the heating element;
 - a conduit configured to direct the gas towards a patient;

a blower disposed in electrical communication with the microprocessor and being capable of advancing the gas at least partially through the conduit;
and

a feedback system configured for controlling a volume of gas being directed towards the patient.

22. The high flow therapy system of Claim 21, further including at least one gas flow sensor disposed in electrical communication with the microprocessor and configured to detect at least one flow characteristic of the gas.
23. The high flow therapy system of Claim 21, further including at least one compressed gas entry port.
24. The high flow therapy system of Claim 21, further including a pulse oximeter.
25. A high flow therapy system, comprising:
- a microprocessor;
 - a heating element disposed in electrical communication with the microprocessor and capable of heating a liquid to create a gas;
 - a humidity chamber disposed in mechanical cooperation with the heating element;
 - a conduit configured to direct the gas towards a patient;
 - at least one proportional valve disposed in electrical communication with the microprocessor and configured to help control the entry and passage of gas; and

a feedback system configured for controlling a volume of gas being directed towards the patient.

26. The high flow therapy system of Claim 25, further including at least one gas flow sensor disposed in electrical communication with the microprocessor and configured to detect at least one flow characteristic of the gas.

27. A method for delivering heated and humidified respiratory gas to a patient, the method comprising the steps of:

providing a high flow therapy device including a heating element capable of heating a liquid to create a gas;

providing a non-sealing respiratory interface disposed in mechanical cooperation with the high flow therapy device and configured to direct the gas towards a patient;

providing a sensor disposed in electrical communication with a microprocessor of the high flow therapy device, the sensor configured to measure a flow rate of the gas delivered to the patient;

delivering gas from the high flow therapy device to a patient; and

measuring the flow rate of the gas delivered to the patient.

28. The method of Claim 27, further including adjusting at least one of the flow rate and the temperature of the gas delivered to the patient.

29. The method of Claim 27, further including determining whether the amount of liquid heatable by the heating element is inadequate for continued use.

30. The method of Claim 29, further including responding to an inadequate amount of liquid by at least one of triggering an auditory or visual signal, adding liquid to the high flow therapy device, adjusting the temperature of the gas delivered to the patient, and adjusting the flow rate of the gas delivered to the patient.

31. A high flow therapy system, comprising:

a microprocessor;

a heating element disposed in electrical communication with the microprocessor and capable of heating a liquid to create a gas;

a humidity chamber disposed in mechanical cooperation with the heating element;

a conduit configured to direct the gas towards a patient interface; and

a saddle disposed in electrical communication with the microprocessor and configured to activate a dry cycle when a portion of at least one of the conduit and a patient interface is engaged therewith.

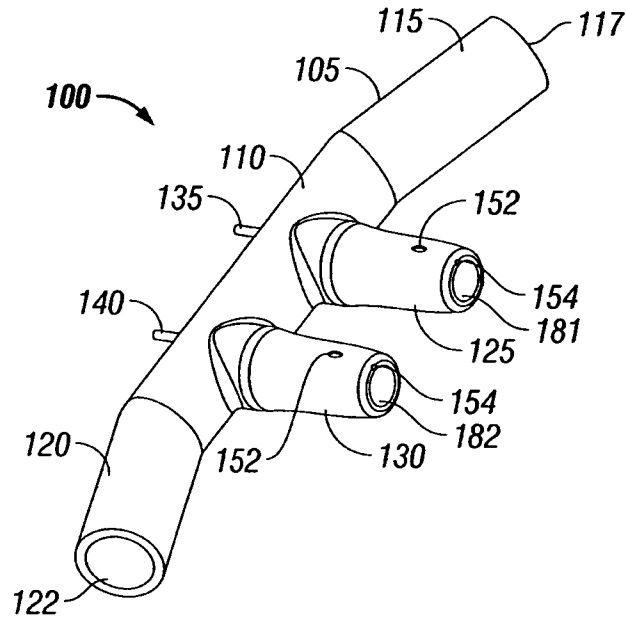


FIG. 1

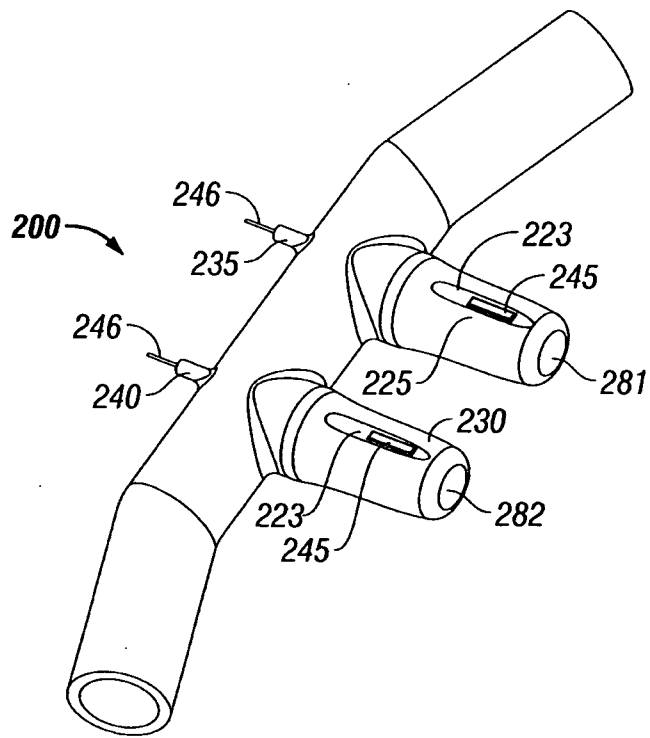


FIG. 2

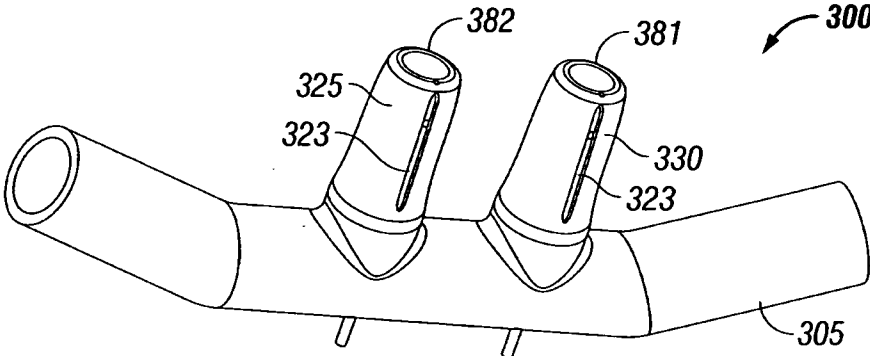


FIG. 3

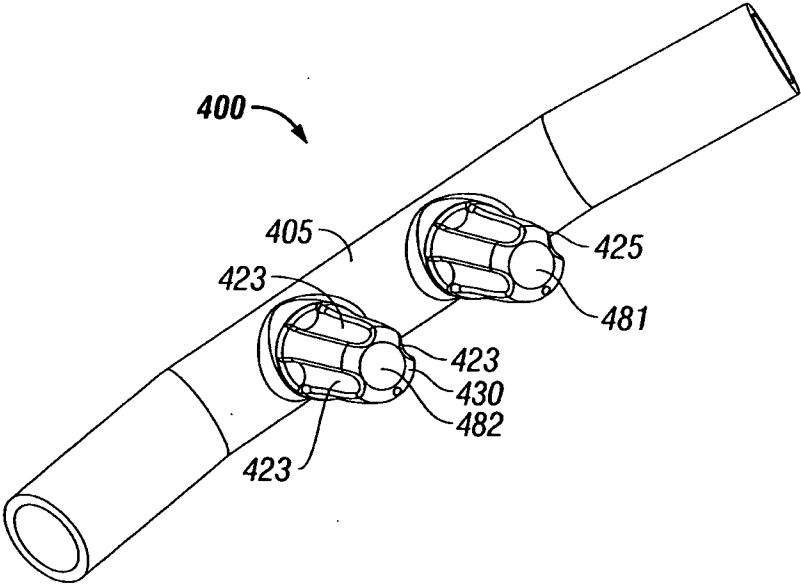


FIG. 4

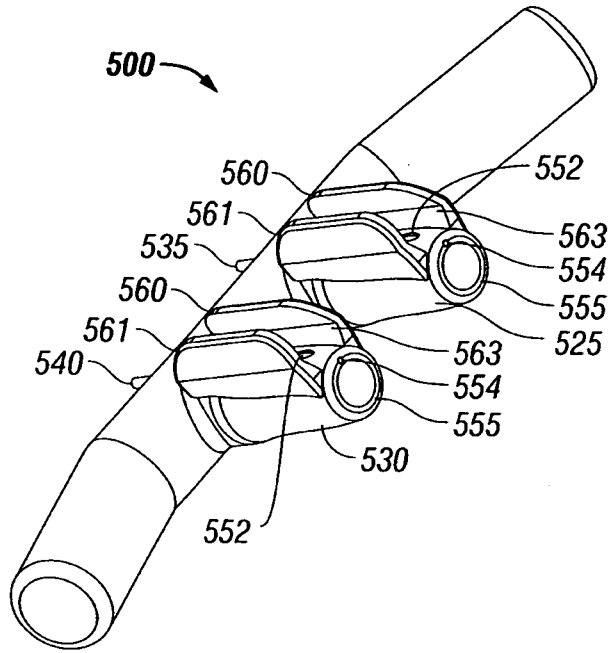


FIG. 5

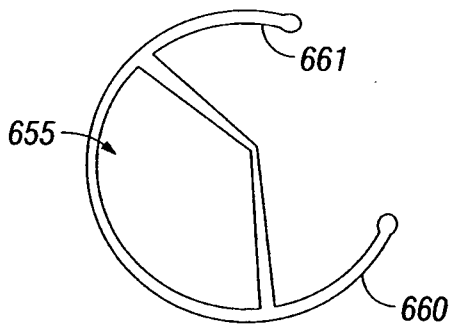


FIG. 6

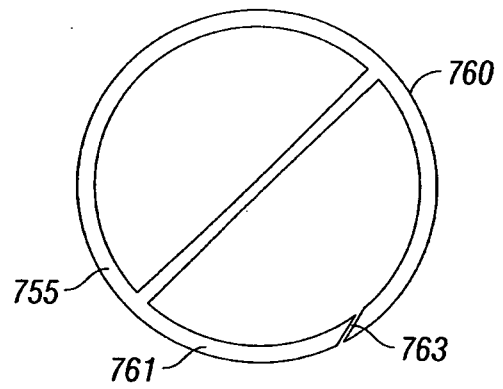


FIG. 7

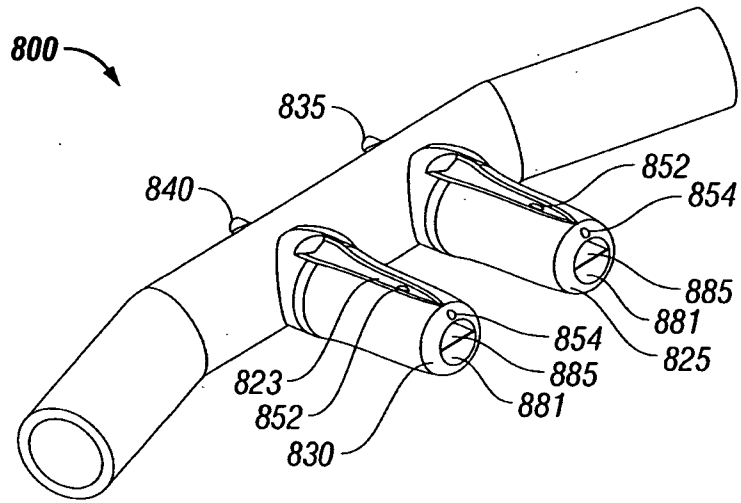


FIG. 8A

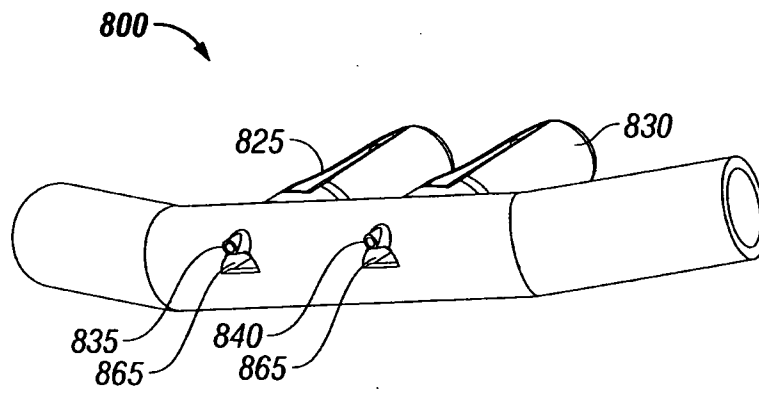


FIG. 8B

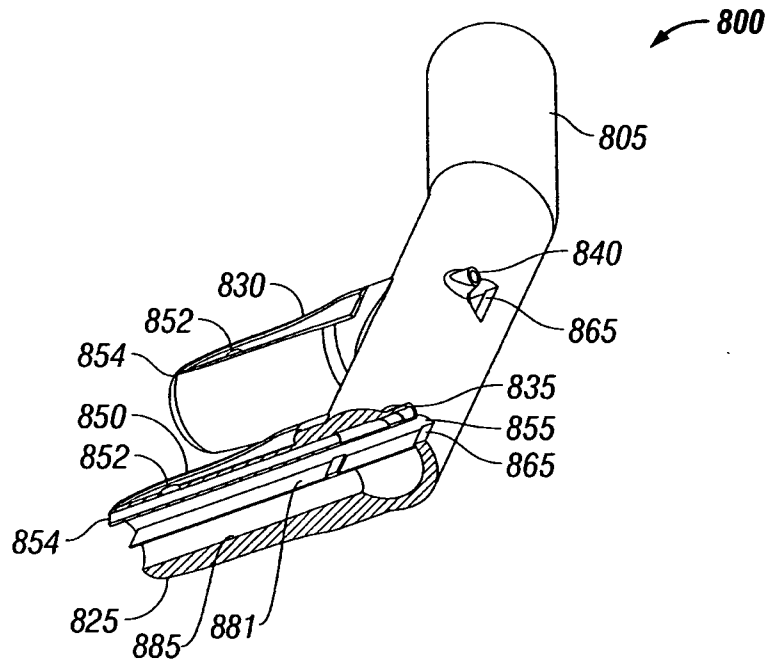


FIG. 8C

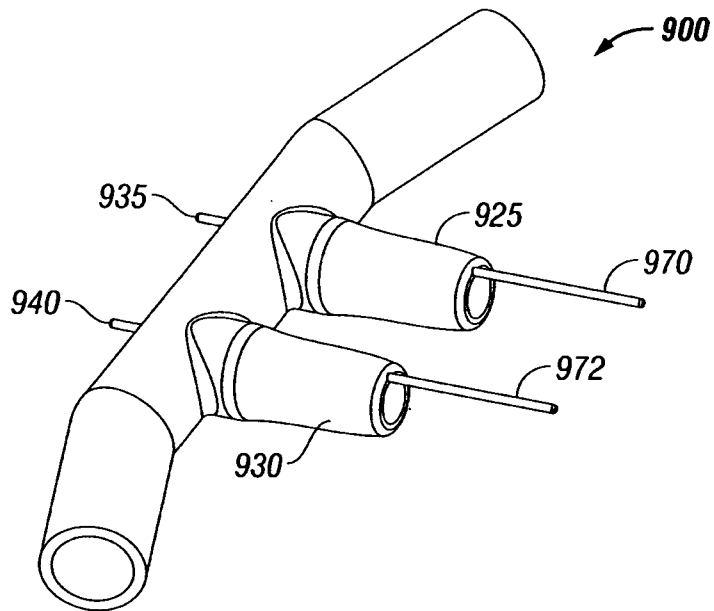


FIG. 9

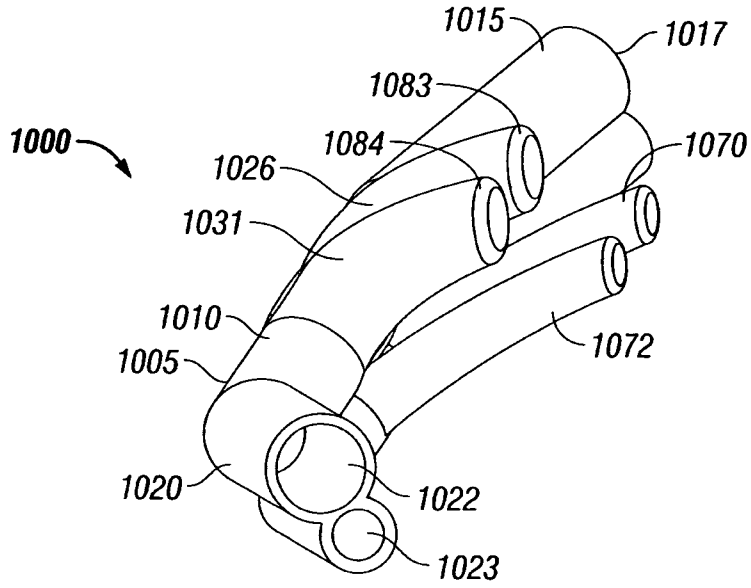


FIG. 10

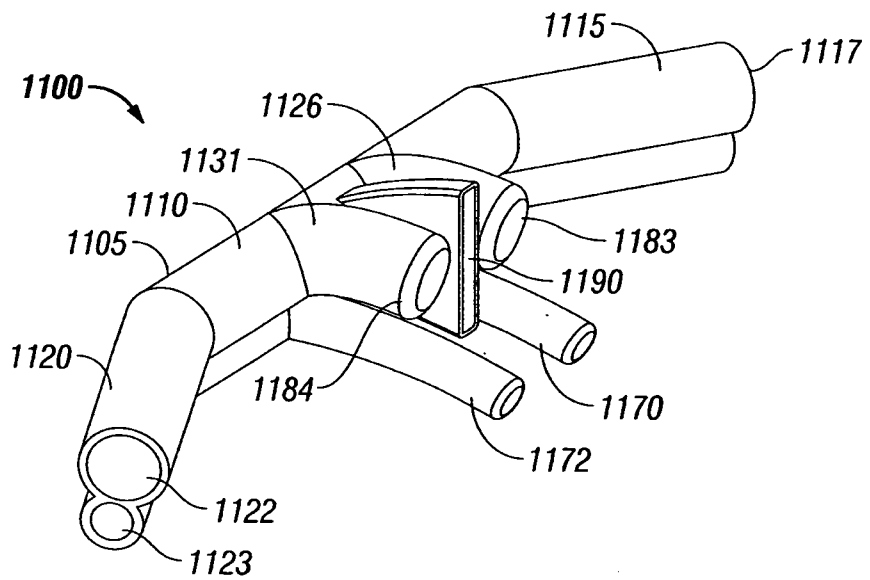


FIG. 11

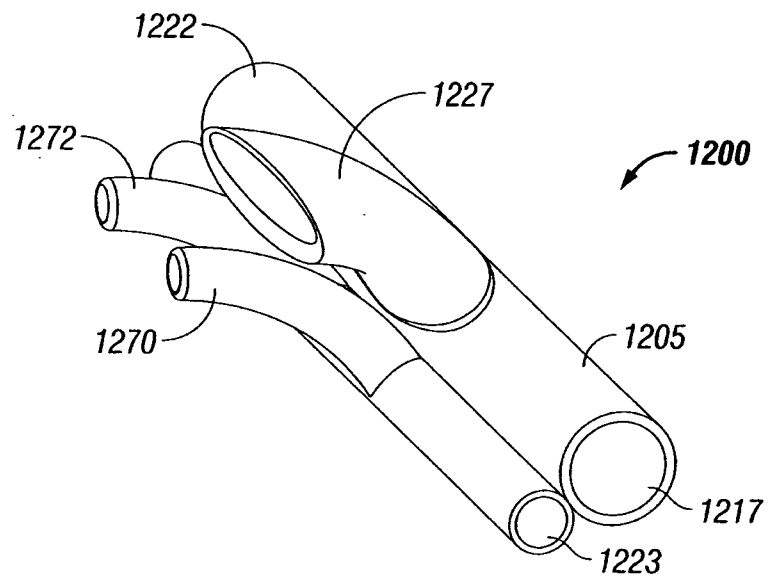


FIG. 12

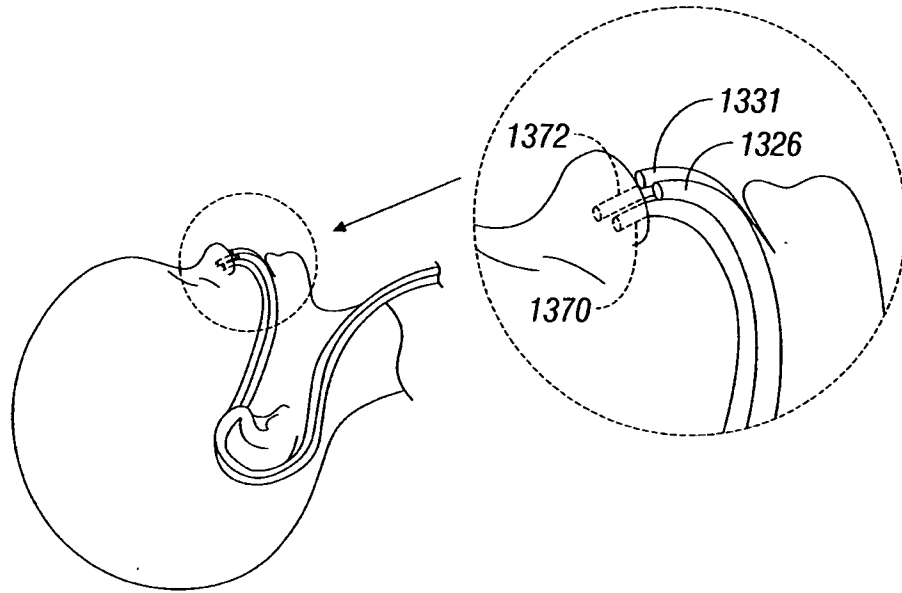


FIG. 13

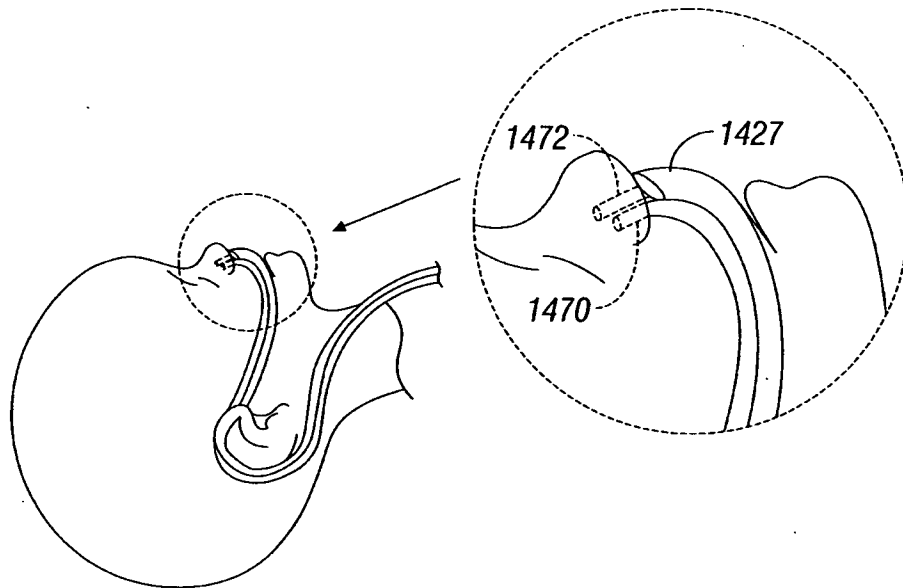


FIG. 14

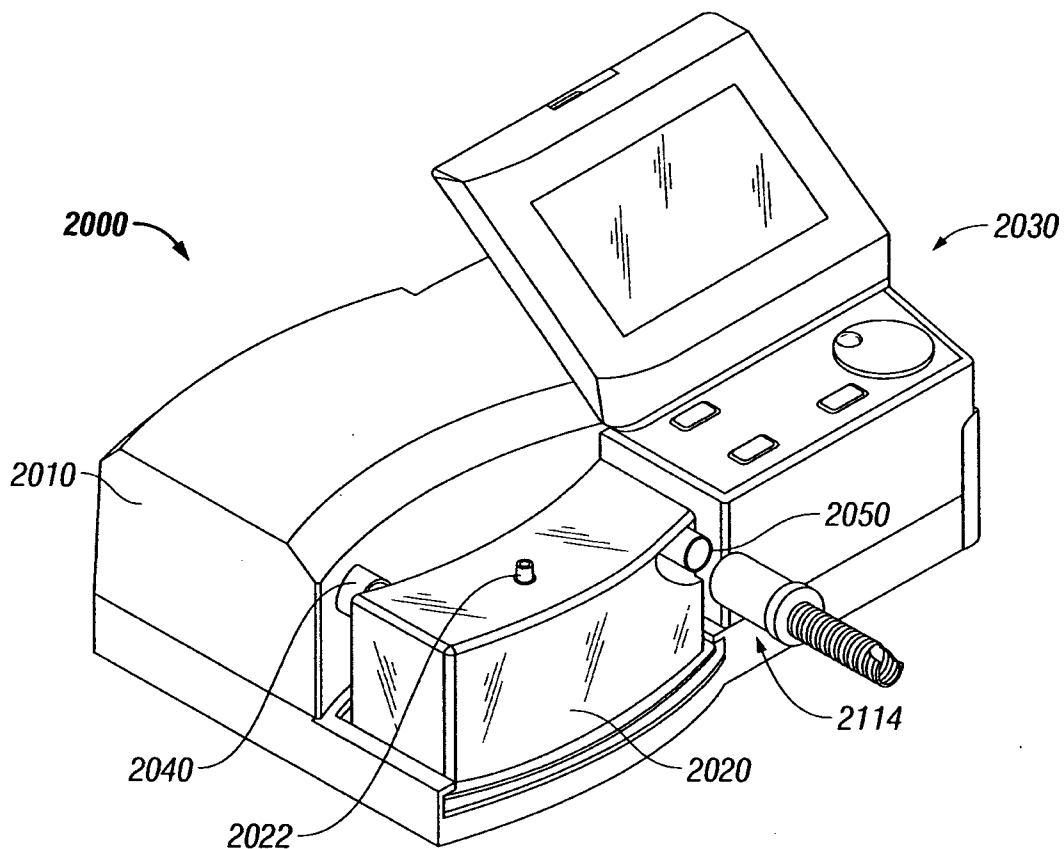


FIG. 15

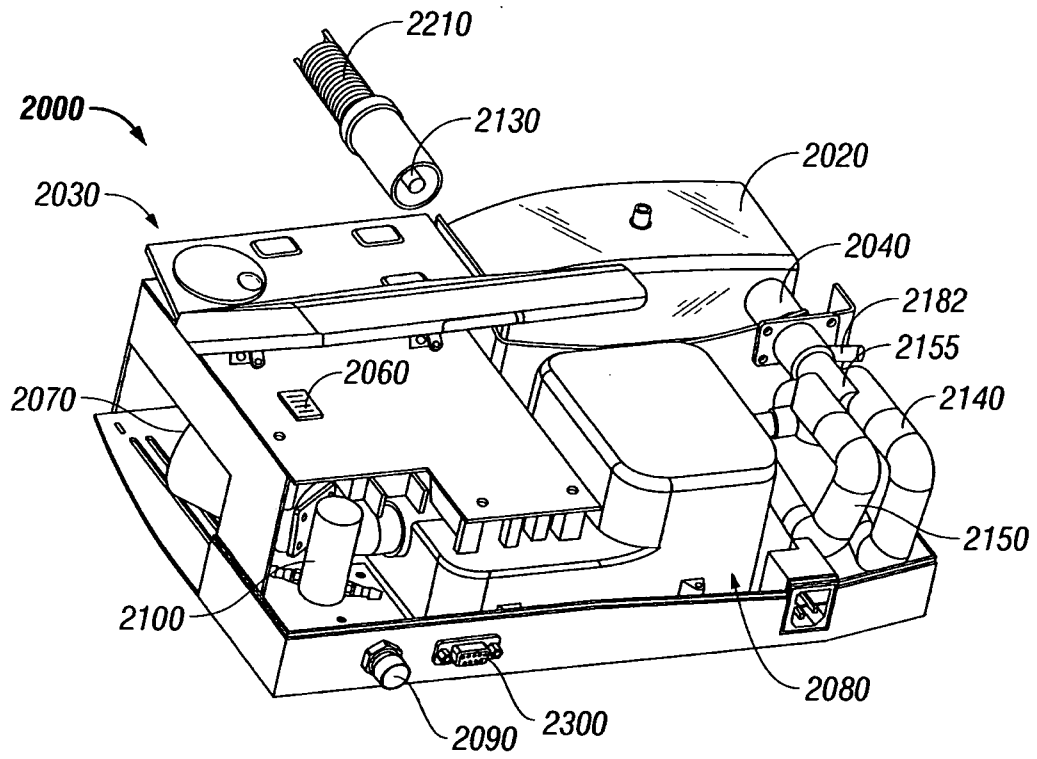


FIG. 16

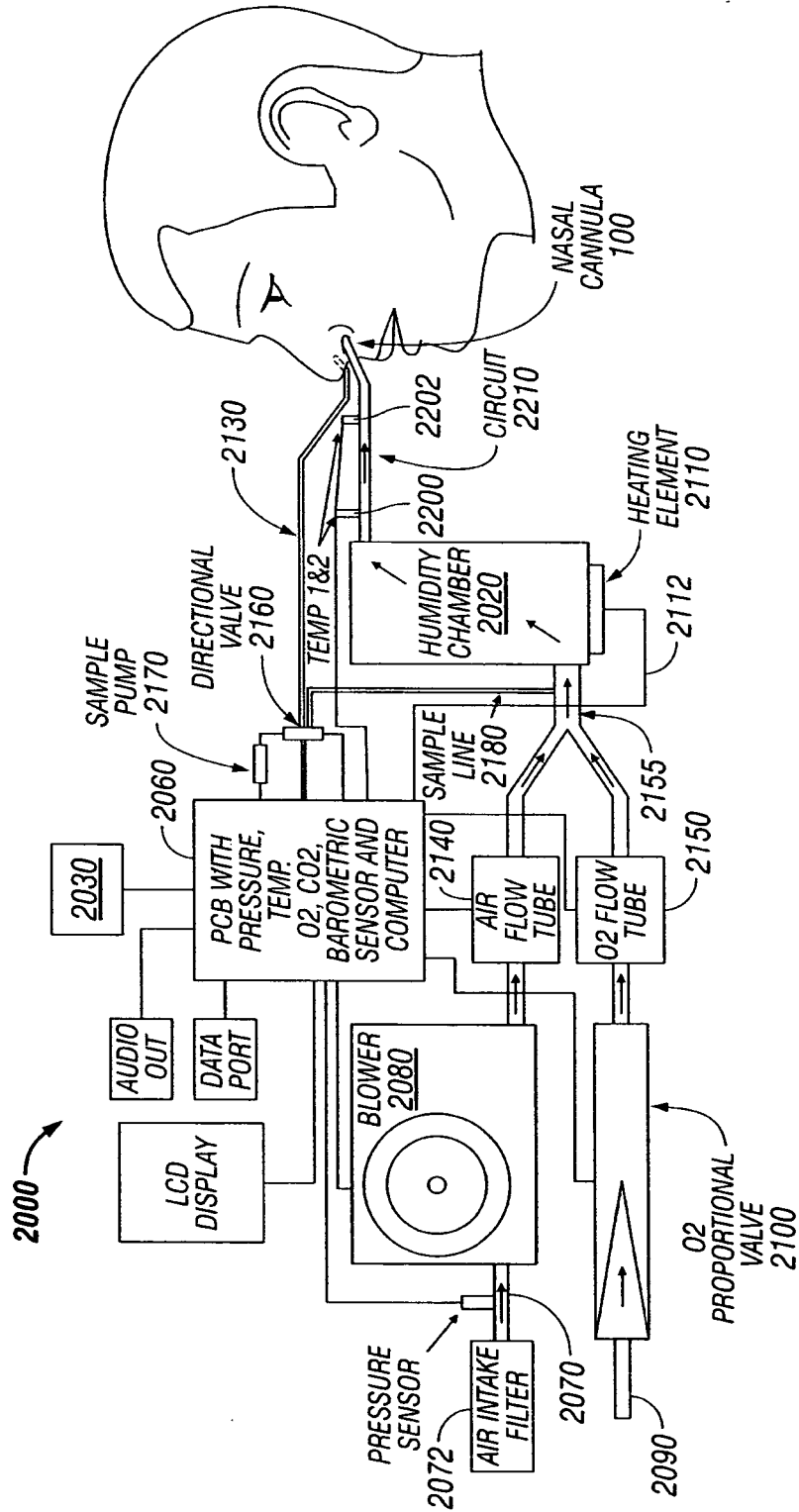


FIG. 17

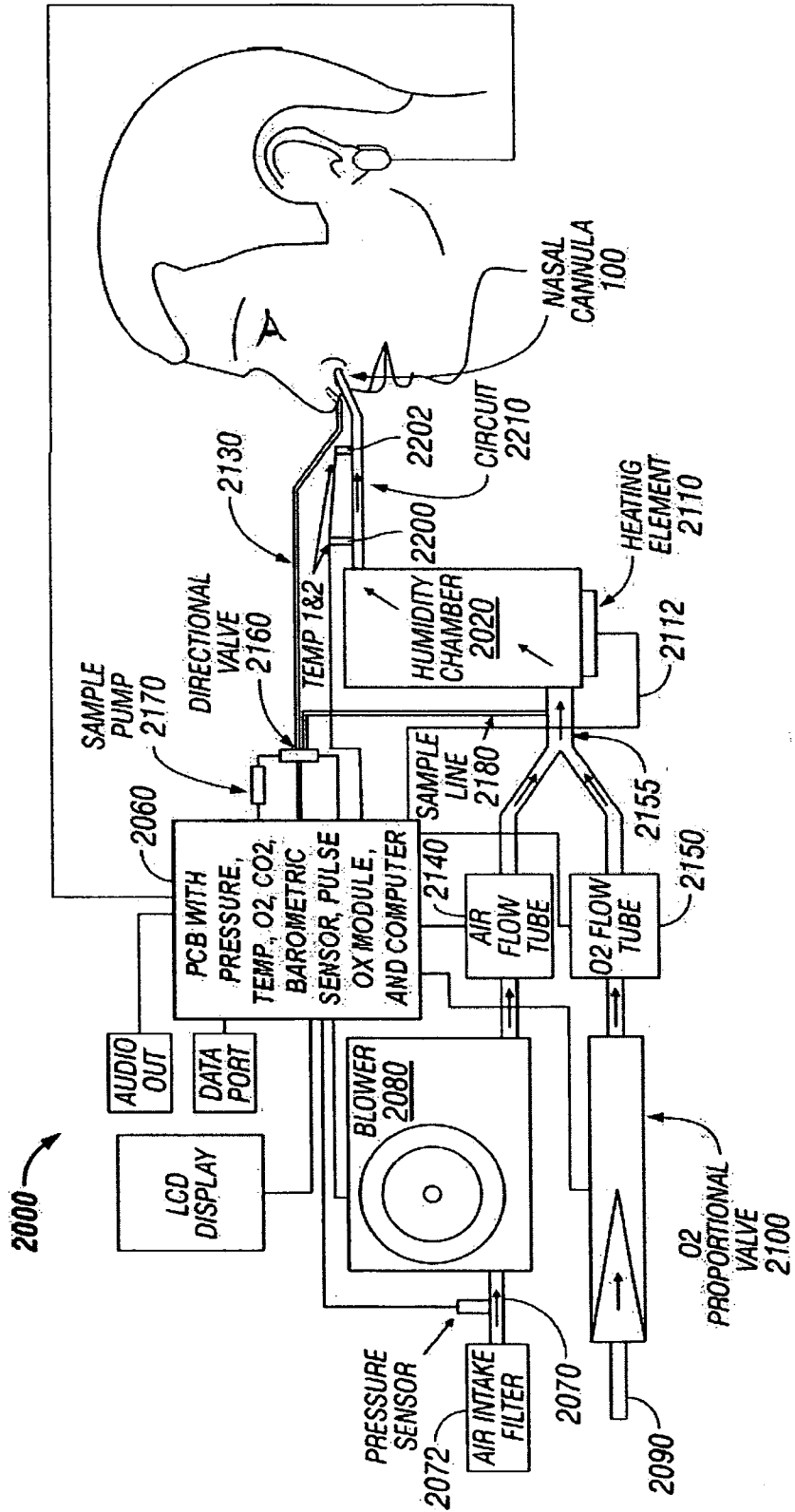


FIG. 17A

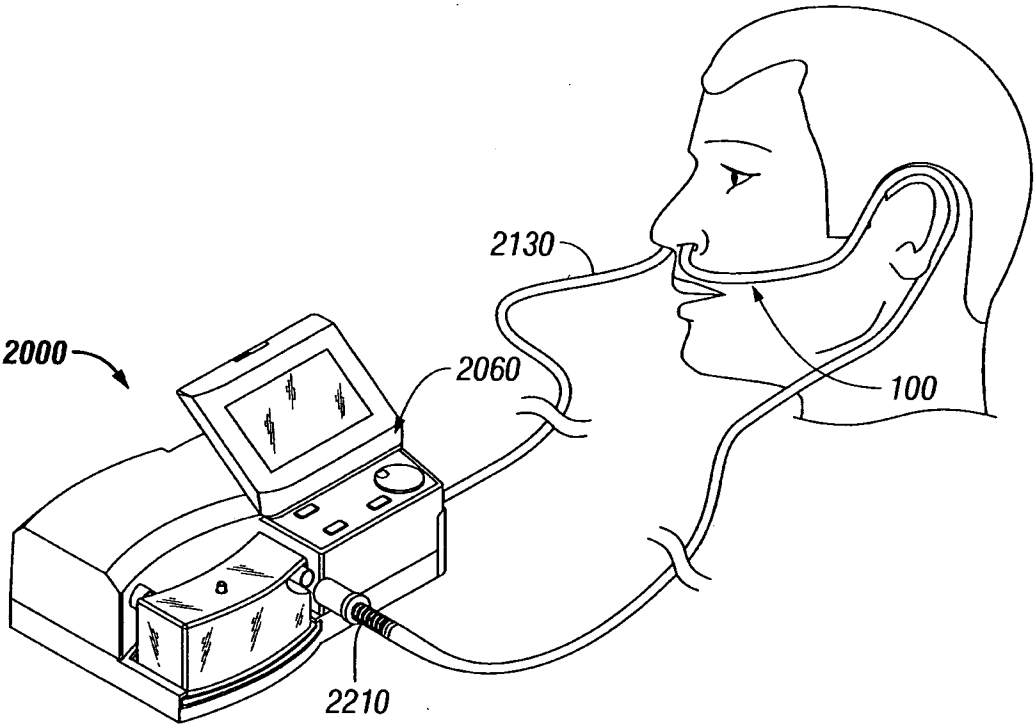


FIG. 18

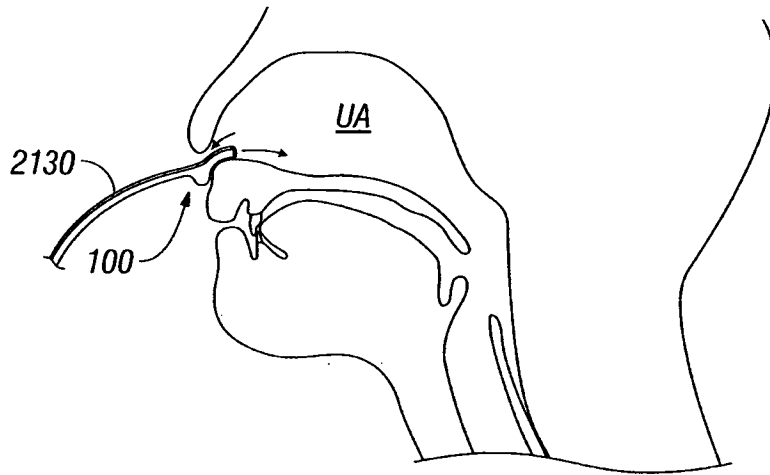


FIG. 19

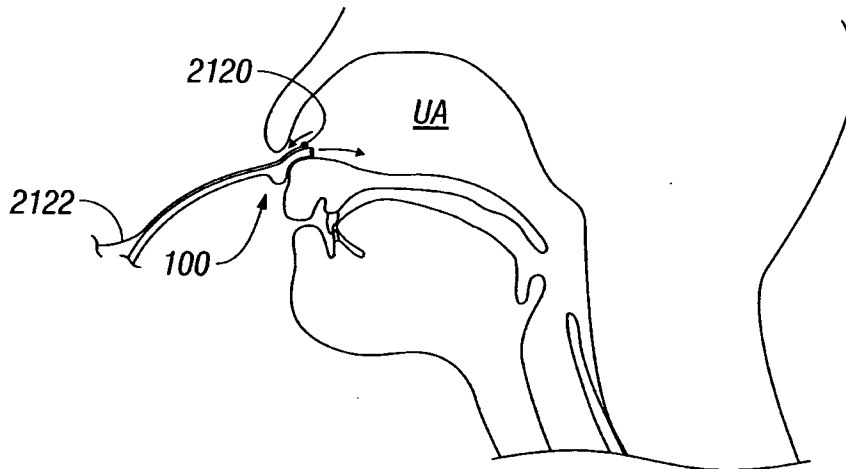


FIG. 20

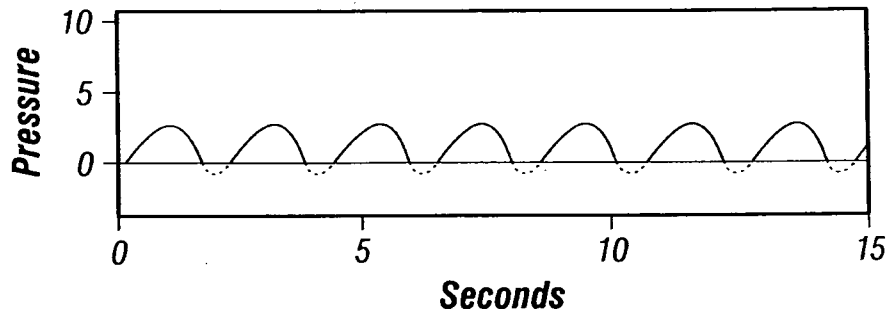


FIG. 21

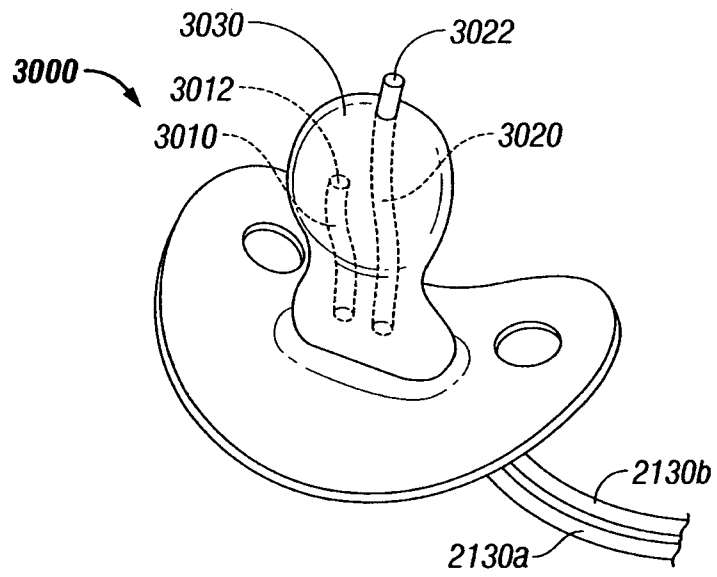


FIG. 22

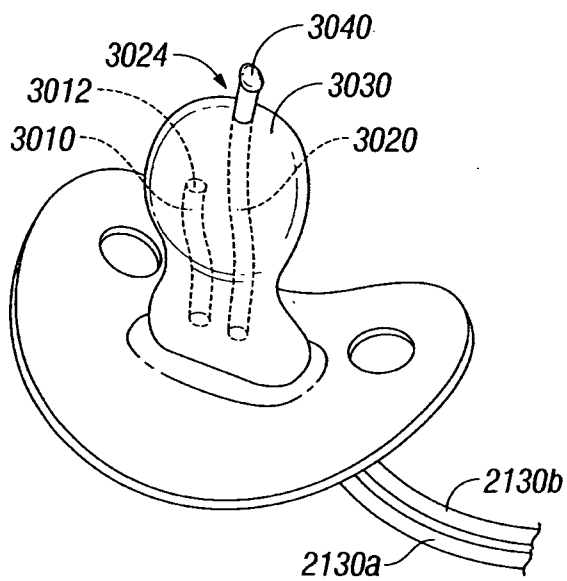


FIG. 23

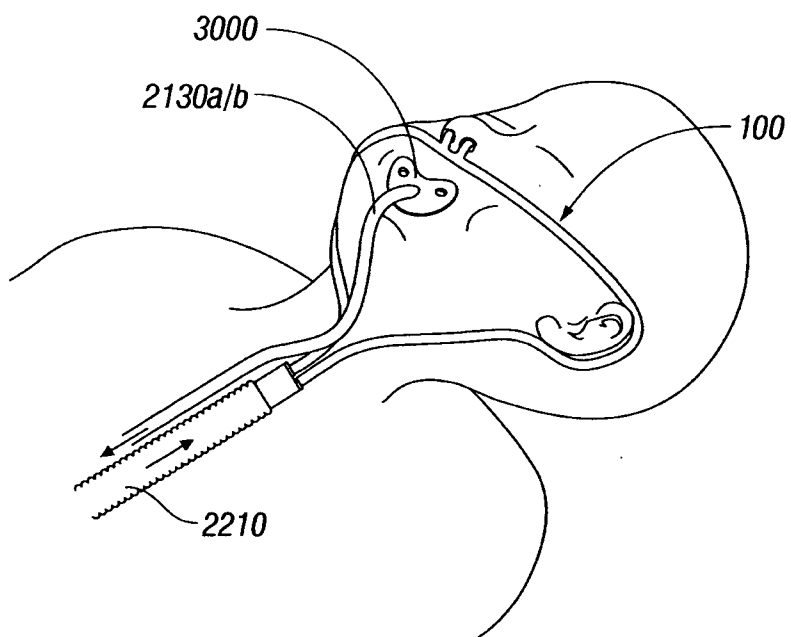


FIG. 24

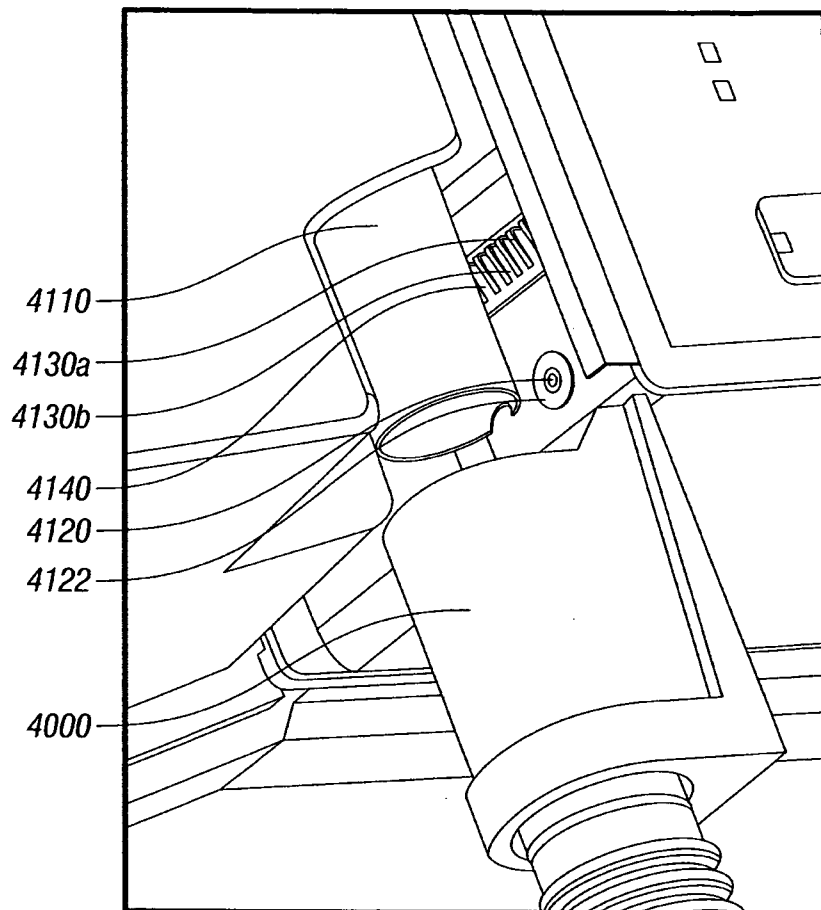


FIG. 25

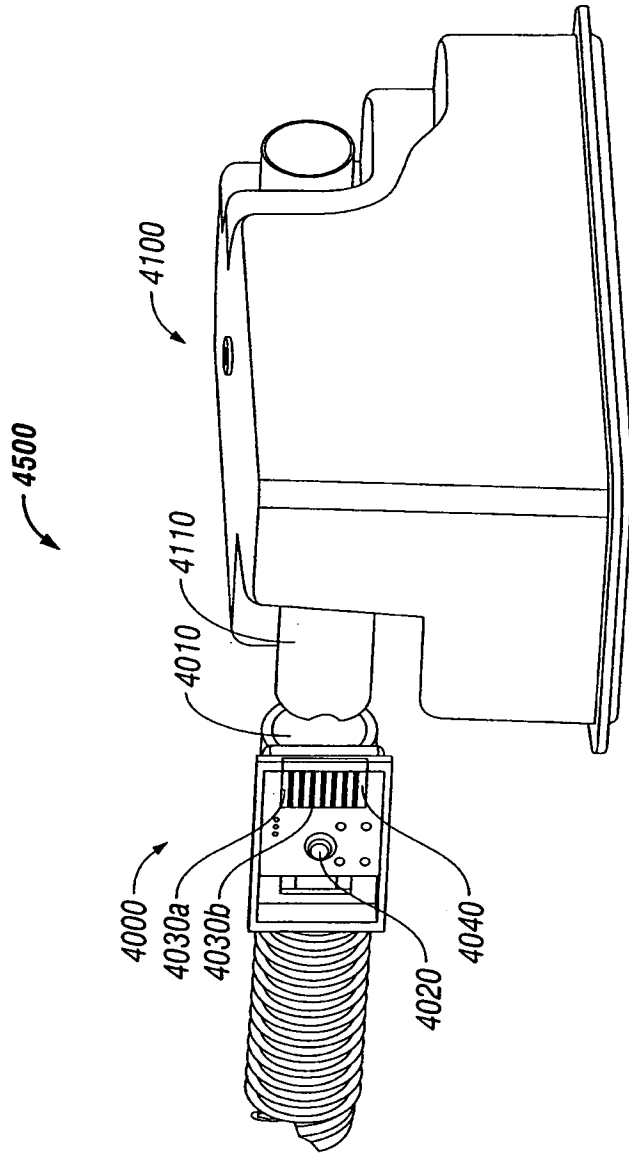


FIG. 26

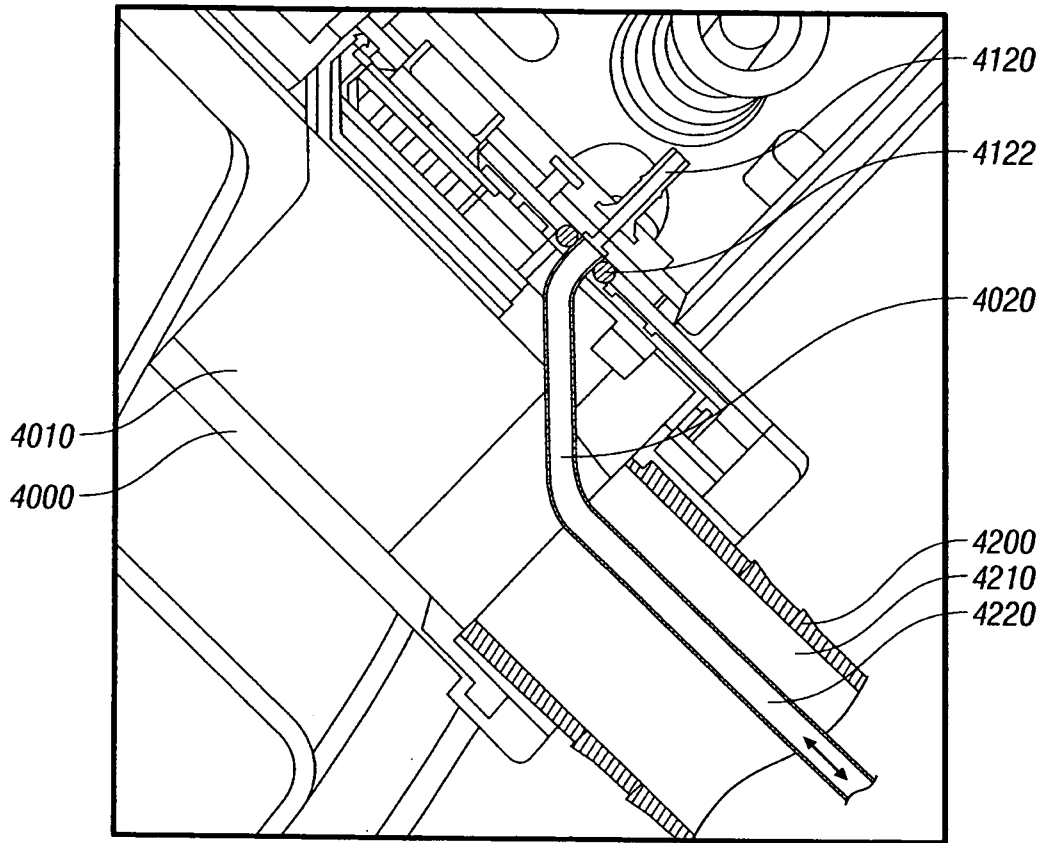


FIG. 27

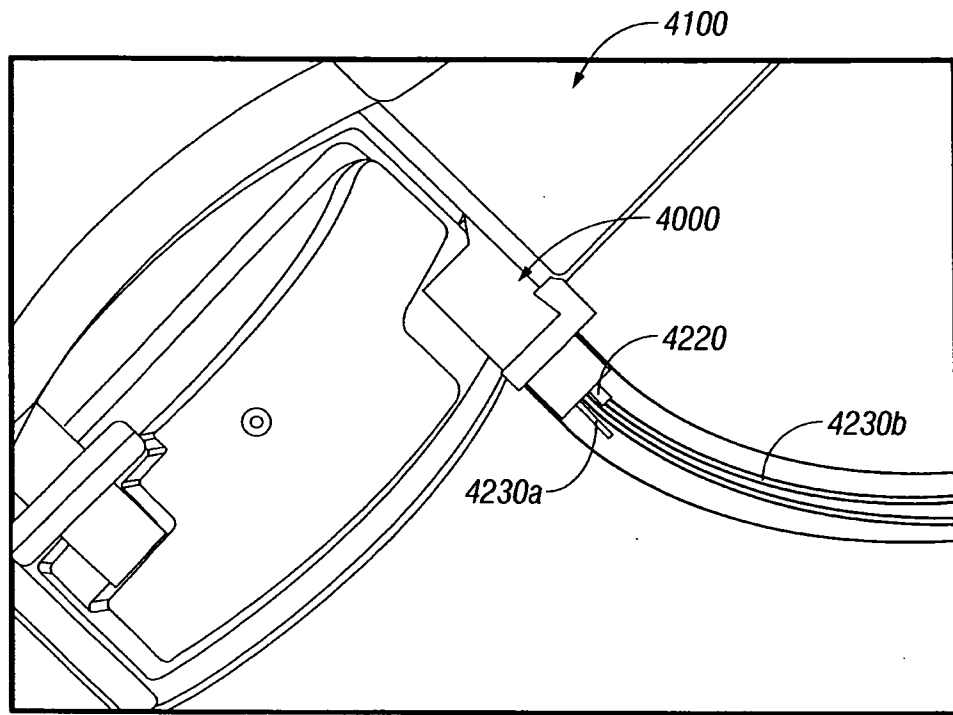


FIG. 28

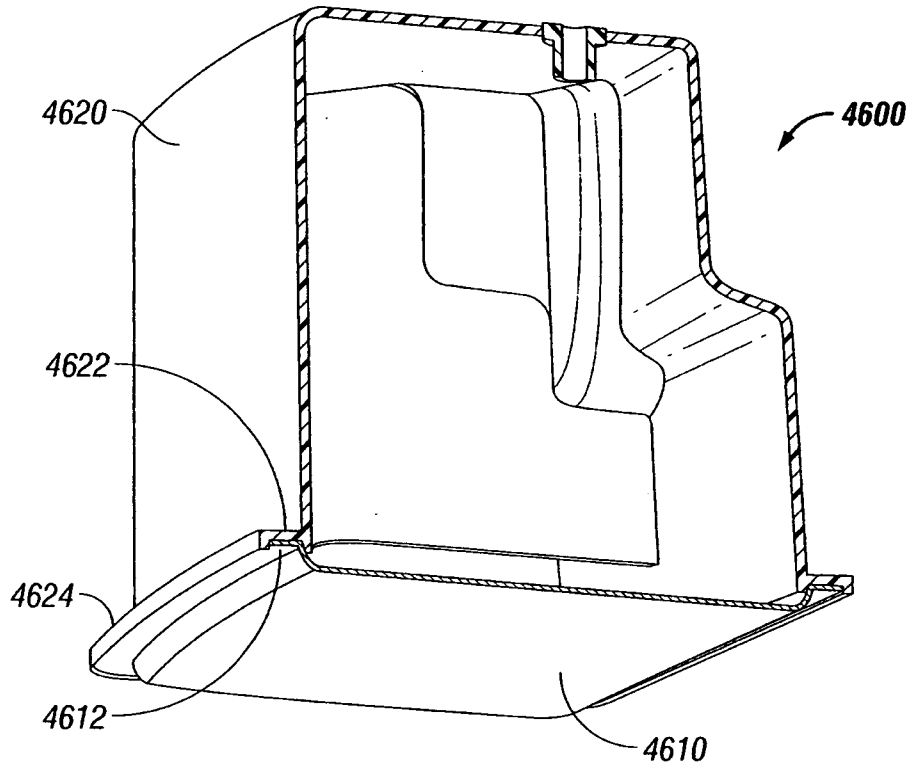


FIG. 29

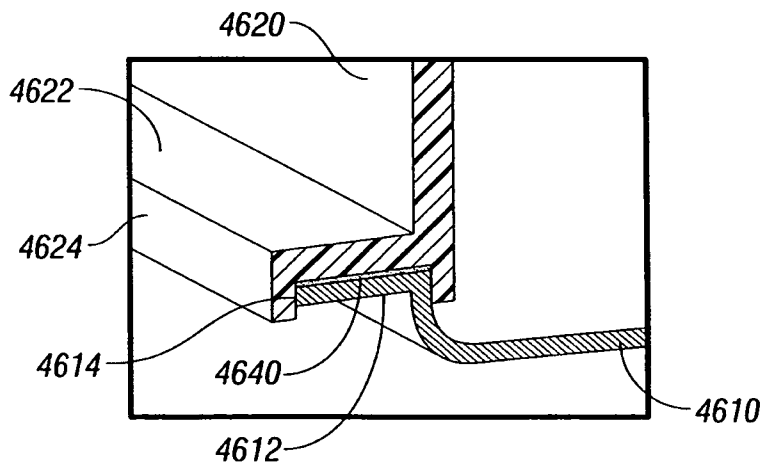


FIG. 29A

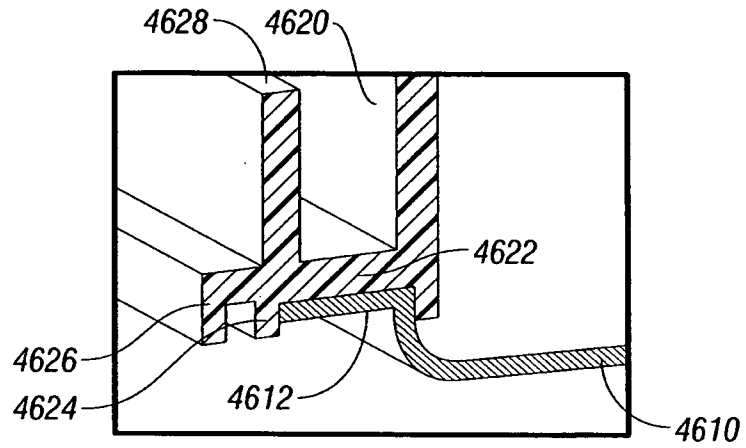


FIG. 29B

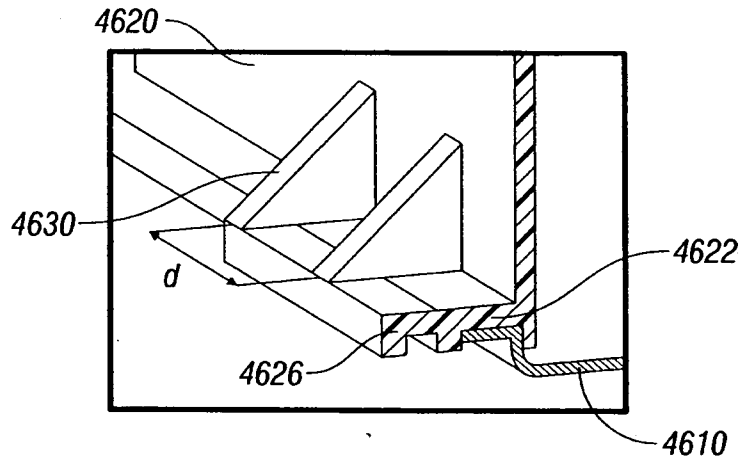


FIG. 29C

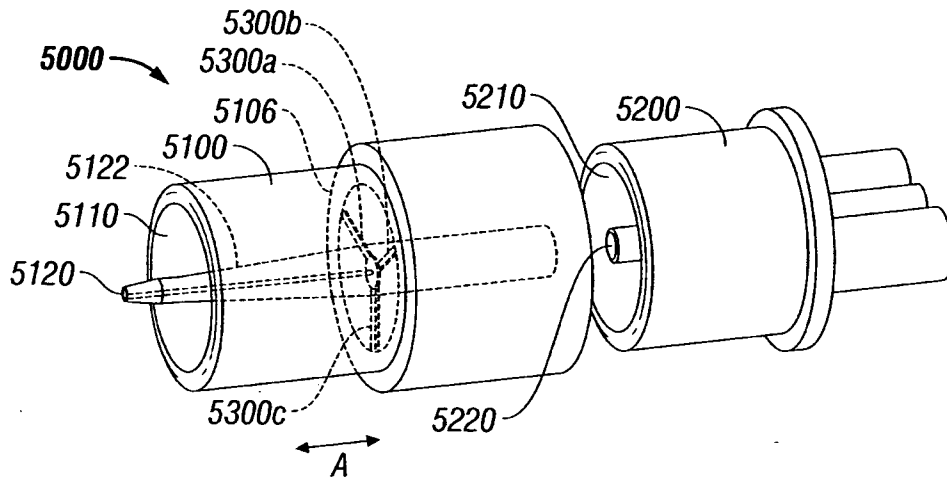


FIG. 30

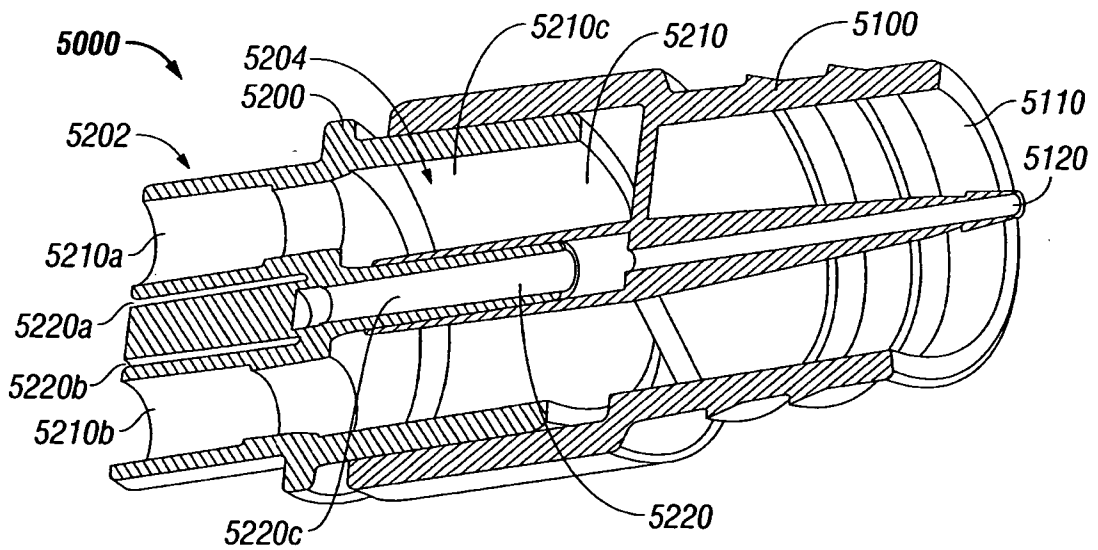


FIG. 31

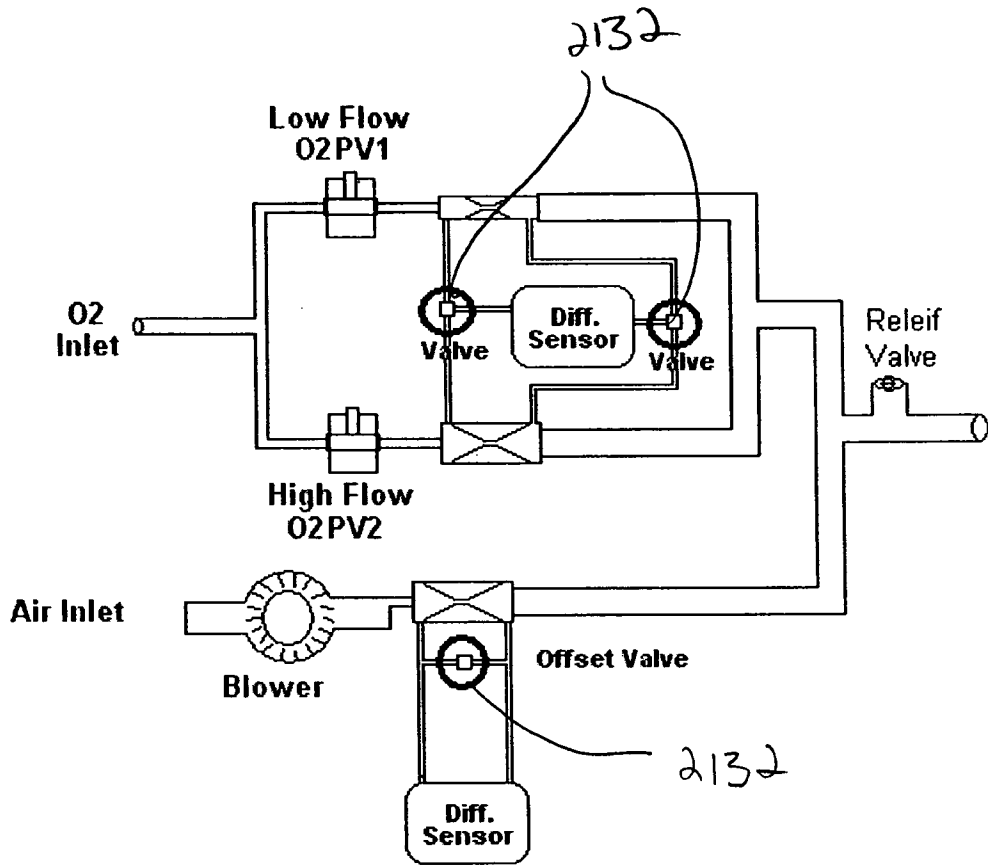


FIG. 32 A

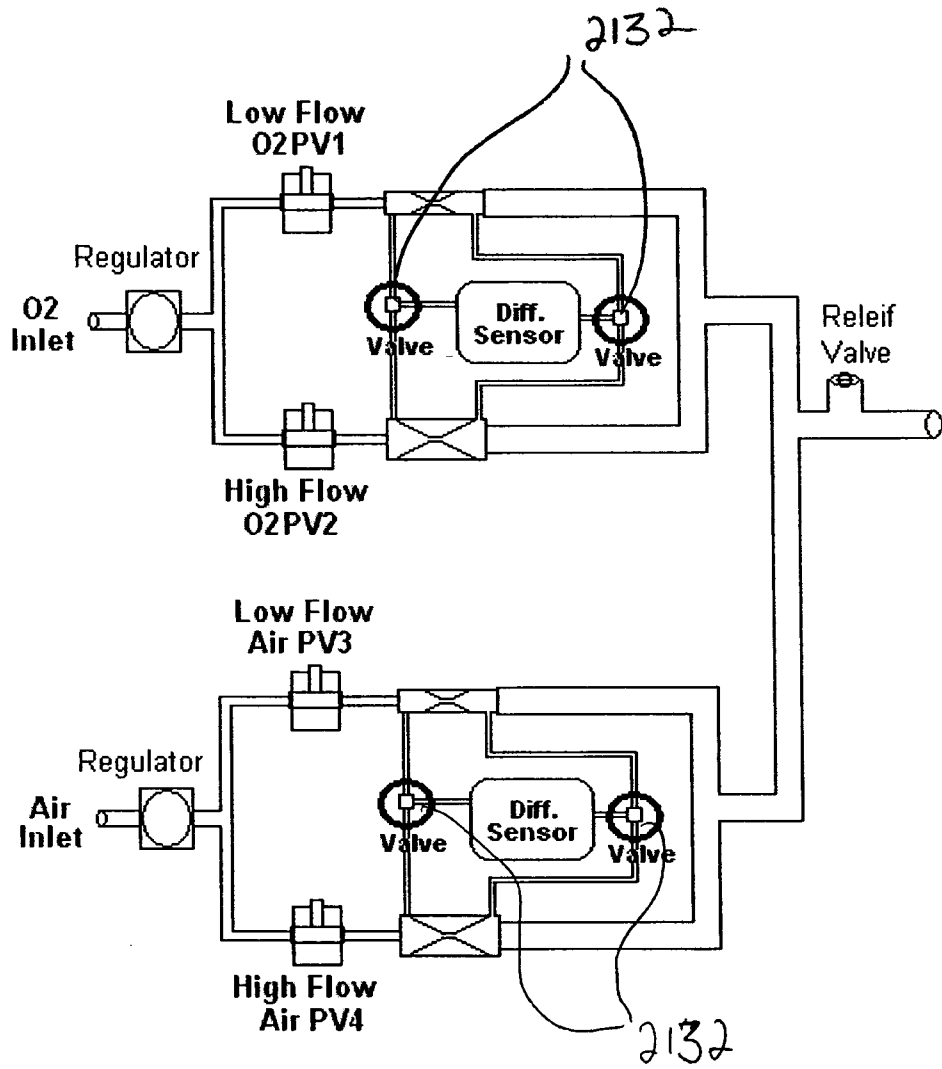


FIG. 32B

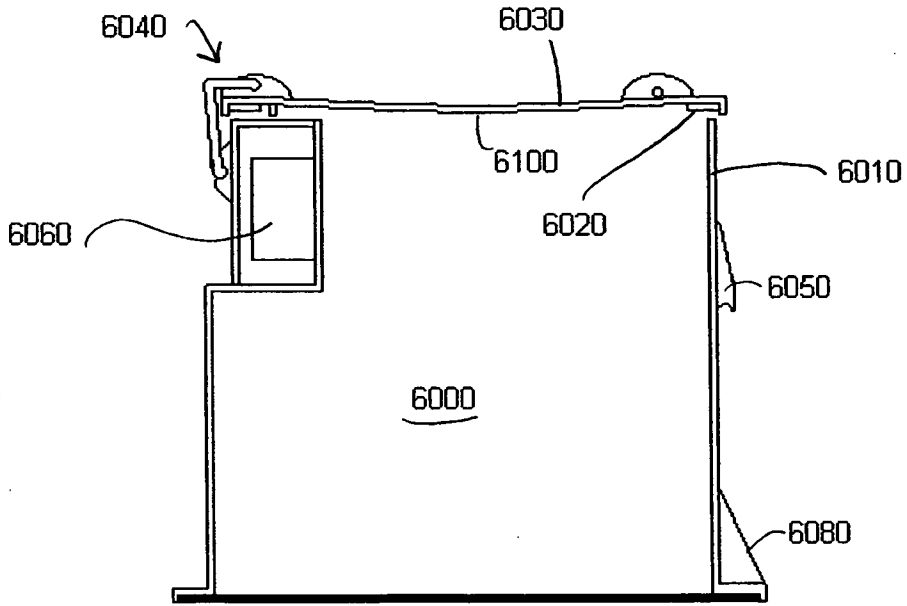


FIG. 33A

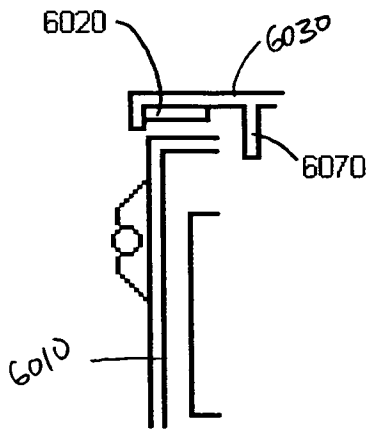


FIG. 33B

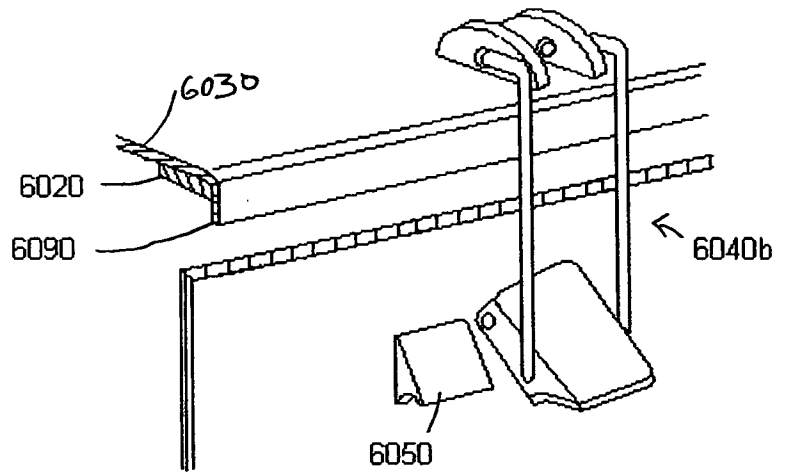


FIG. 33C

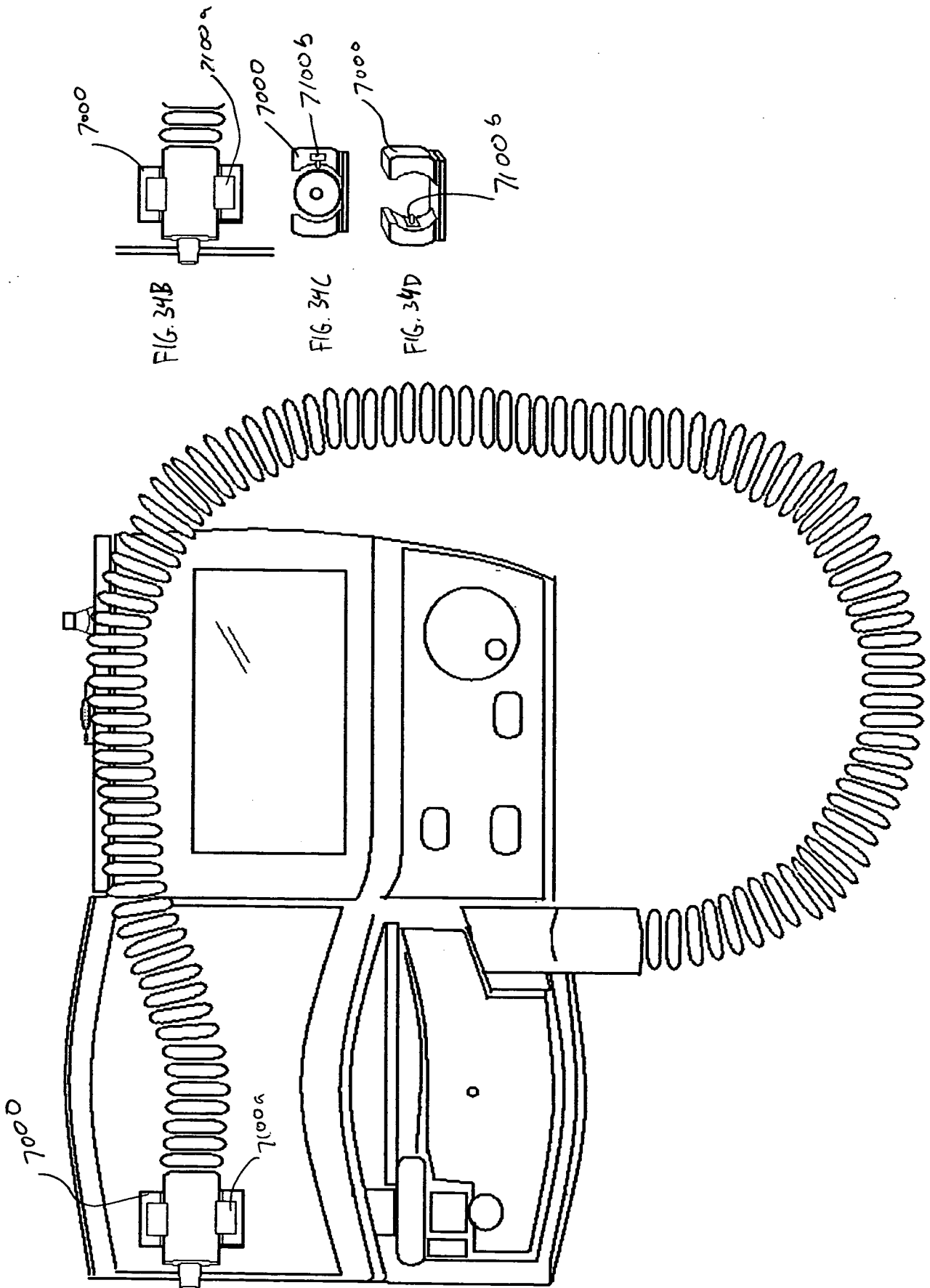


FIG. 34A

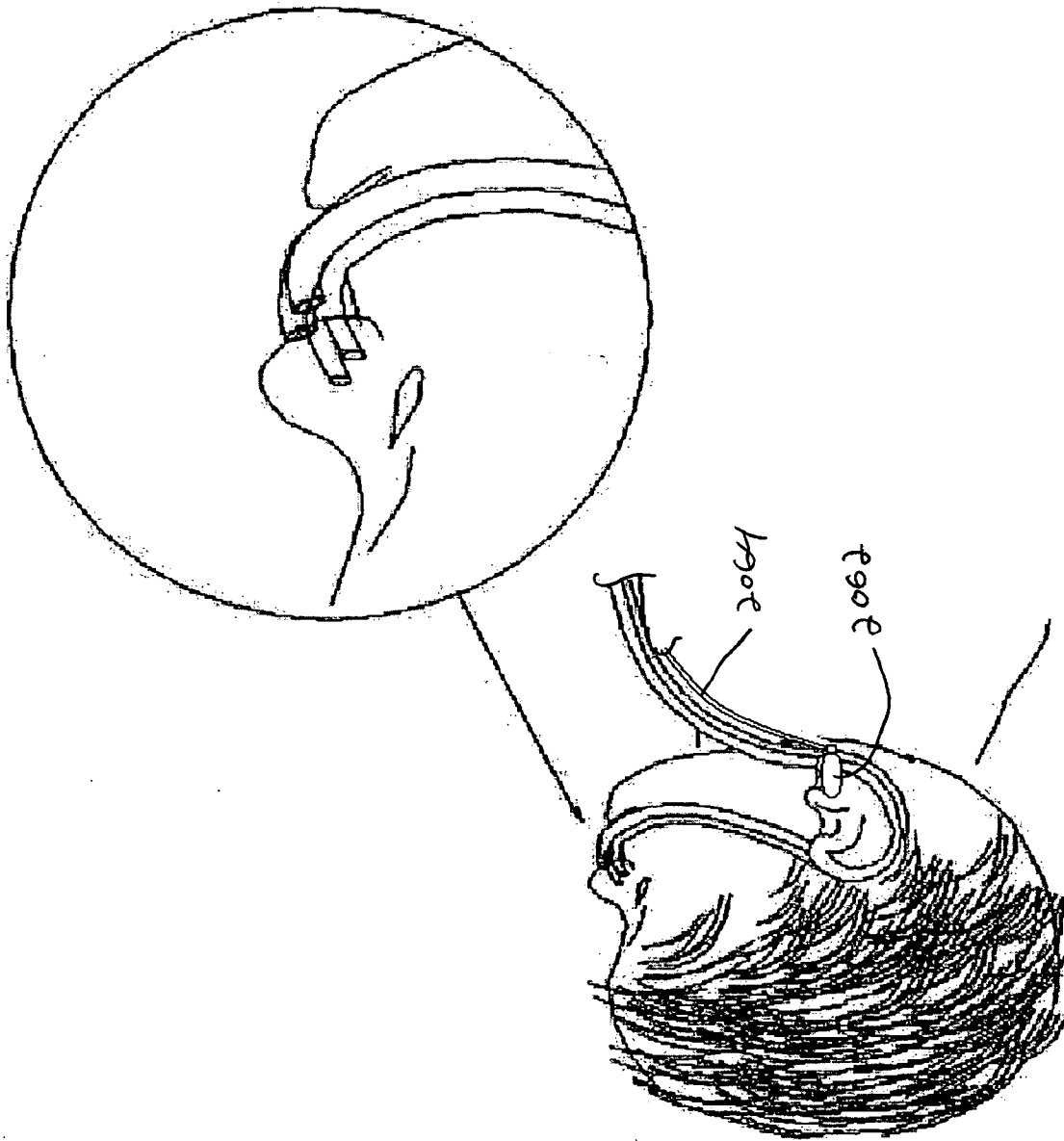


FIG. 35