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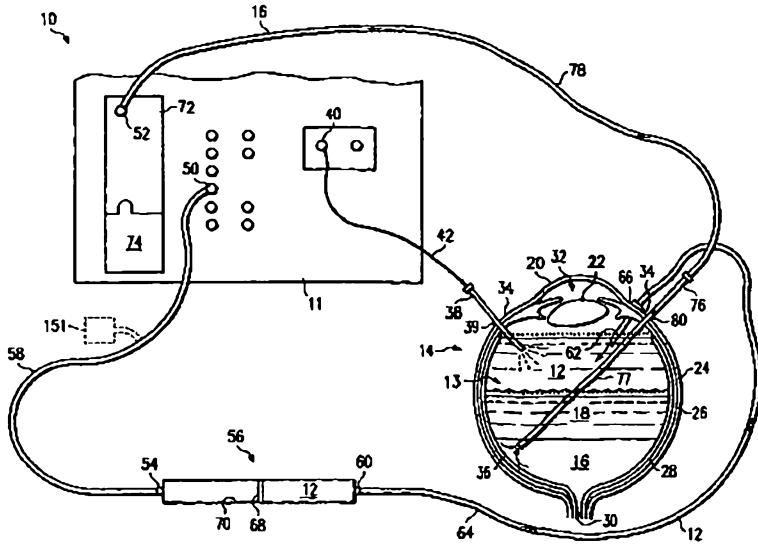
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(54) Title: SIMULTANEOUS INJECTION AND ASPIRATION OF VISCOUS SURGICAL FLUIDS



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(57) Abstract: A method of injecting a first viscous fluid into a target tissue simultaneous with aspirating a second viscous fluid from the target tissue is disclosed. A surgical system is provided that is capable of supplying pneumatic pressure and vacuum. A first viscous fluid is injected into the target tissue using pneumatic pressure from the system. A mode of operation of the system is changed to provide vacuum and pneumatic pressure. The second viscous fluid is aspirated from the target tissue using vacuum from the system, and the pneumatic pressure remains substantially constant during aspiration. An improved foot pedal for controlling the simultaneous injection and aspiration of viscous fluids is also disclosed.

SIMULTANEOUS INJECTION AND ASPIRATION OF VISCOUS SURGICAL FLUIDS

Field of the Invention

The present invention generally pertains to apparatus and methods for providing simultaneous viscous fluid injection and aspiration in a surgical system. More particularly, but not by way of limitation, the present invention pertains to apparatus and methods for injecting a long-term viscous fluid tamponade into the posterior segment of the eye while simultaneously aspirating a short-term viscous fluid tamponade out of the eye during vitreoretinal surgery.

Description of the Related Art

In a healthy human eye, the retina is physically attached to the choroid in a generally circumferential manner behind the pars plana. The vitreous humor, a transparent jelly-like material that fills the posterior segment of the eye, helps to cause the remainder of the retina to lie against, but not physically attach, to the choroid. A helpful analogy is to imagine the choroid as the walls of a swimming pool. The retina is like a wallpaper that is pressed against the walls of the swimming pool by the water in the pool, but is only physically attached to the walls at the top of the pool.

Sometimes a portion of the retina becomes detached from the choroid. Other times a portion of the retina may tear, allowing aqueous humor, and sometimes vitreous, to flow between the retina and the choroid. Both of these conditions result in a loss of vision.

To surgically repair these conditions, a surgeon typically inserts a vitrectomy probe into the posterior segment of the eye via an incision through the sclera in the pars plana. Such an incision is called a sclerotomy. The surgeon typically also inserts a fiber optic light source and an infusion cannula into the eye via similar incisions, and may sometimes substitute an aspiration probe for the vitrectomy probe. While viewing the posterior segment under a microscope and with the aid of the fiber optic light source, the surgeon cuts and aspirates away vitreous using the vitrectomy probe to gain access to the retinal detachment or tear. The surgeon may also use the vitrectomy probe, scissors, a pick, and/or forceps to remove any membrane that has contributed to the retinal detachment or tear. During this portion of the surgery, a saline solution is typically

infused into the eye via the infusion cannula to maintain the appropriate intraocular pressure.

5 Next, many surgeons inject a perfluorocarbon liquid into the posterior segment of the eye to cause the detached or torn portion of the retina to flatten against the choroid in the proper location. Once the detached or torn portion of the retina is properly located, the surgeon uses a diathermy probe or a laser to fuse portions of the detached retina in place.

10 Unfortunately, perfluorocarbon liquids are toxic when left in the eye for a period of weeks. Since a retinal tear or detachment takes a period of weeks to re-attach after the above-described surgical procedure, the short-term perfluorocarbon liquid tamponade must be removed from the eye at the latter portion of the surgical procedure and replaced with a long-term tamponade. This long-term tamponade can be an air/gas mixture or a viscous fluid, such as silicone oil. If silicone oil is used, it too must be extracted from the eye after the retina re-attaches because it is toxic when left in the eye for a period of 15 months.

A need exists in vitreoretinal surgery for an improved surgical system and a method that provides long-term tamponading of the retina. The system and method should be easy for the surgeon to use, should maximize patient safety, and should be economically feasible.

20 **Summary of the Invention**

In a first aspect of the present invention, there is provided a method of injecting a first retinal tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment, including the 25 steps of:

providing a surgical system capable of supplying pneumatic pressure and vacuum; injecting said first retinal tamponading fluid into said posterior segment using pneumatic pressure from said system; changing a mode of operation of said system to provide vacuum and pneumatic pressure; and



aspirating said second retinal tamponading fluid from said posterior segment using vacuum from said system, wherein said pneumatic pressure remains substantially constant during said aspirating step.

One aspect of the present invention provides a method of injecting a first viscous fluid into a target tissue simultaneous with aspirating a second viscous fluid from the target tissue. A surgical system is provided that is capable of supplying pneumatic pressure and vacuum. A first viscous fluid is injected into the target tissue using pneumatic pressure from the system. A mode of operation of the system is changed to provide vacuum and pneumatic pressure. The second viscous fluid is aspirated from the target tissue using vacuum from the system.

In another aspect of the invention there is provided a surgical system for injecting a first retinal tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment, said posterior segment having a volume, including:

an assembly capable of supplying pneumatic pressure and vacuum;
a syringe; and
tubing fluidly coupling said syringe to said assembly;
wherein a first volume of air in said tubing and said syringe is greater than said volume of said posterior segment.

In another aspect, the present invention provides a surgical system for injecting a first viscous fluid into a target tissue simultaneous with aspirating a second viscous fluid from the target tissue. The surgical system includes an assembly capable of supplying pneumatic pressure and vacuum, a syringe, and tubing fluidly coupling the syringe to the assembly. A first volume of air in the tubing and the syringe is greater than a second volume of the target tissue.

In a further aspect, the present invention provides a surgical system for injecting a first viscous fluid into a target tissue simultaneous with aspirating a second viscous fluid from the target tissue. The surgical system includes an assembly capable of supplying pneumatic pressure and vacuum to at least one microsurgical instrument, and a foot pedal operatively coupled to the assembly. The foot pedal includes a first range of motion in a



generally vertical plane in which the assembly supplies proportional pneumatic pressure, and a second range of motion in a generally vertical plane in which the assembly supplies a substantially constant pneumatic pressure and proportional vacuum.

In another aspect of the present invention there is provided a surgical system for injecting a first retinal tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment, said posterior segment having a volume, including:

a single pneumatic assembly capable of supplying pneumatic pressure and vacuum, said assembly including a reservoir;

10 a syringe having:

a hollow bore with a first end and a second end; and

15 a plunger movably disposed in said hollow bore between said first end and said second end; and

tubing fluidly coupling said first end of said hollow bore to said reservoir;

wherein a volume of said reservoir, said tubing, and said hollow bore on a side of said plunger proximate said first end is greater than said volume of said posterior segment.

Brief Description of the Drawings

For a more complete understanding of the present invention, and for further objects and advantages thereof, reference is made to the following description taken in conjunction with the accompanying drawings in which:

20 FIG. 1 is a schematic, fragmentary, partially sectional illustration of a surgical system for injecting a viscous fluid into a human eye while simultaneously aspirating a second viscous fluid from the eye according to a preferred embodiment of the present invention;

25 FIG. 2 is a block diagram of certain portions of the electronic and pneumatic sub-assemblies of the surgical system of FIG. 1;

FIG. 3 shows a preferred embodiment of a pneumatic reservoir of the surgical system of FIG. 1;

30 FIG. 4 is a schematic illustration of a preferred embodiment of a foot pedal of the surgical system of FIG. 1; and



FIG. 5 is a graphic illustration of the change in injection pressure in the surgical system of FIG. 1.

Detailed Description of the Preferred Embodiments

5 The preferred embodiments of the present invention and their advantages are best understood by referring to FIGS. 1 through 5 of the drawings, like numerals being used for like and corresponding parts of the various drawings.

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FIG. 1 shows a schematic illustration of a surgical system 10 injecting a viscous fluid 12 into a posterior segment 13 of a human eye 14 while simultaneously aspirating a second viscous fluid 16 out of eye 14 according to a preferred method of the present invention. Surgical system 10 is preferably a conventional surgical system capable of performing vitreoretinal surgery that has been modified according to the present invention. An exemplary surgical system 10 suitable for such modification is the Accurus® surgical system sold by Alcon Laboratories, Inc. When surgical system 10 is used to perform a "fluid/fluid exchange" as a portion of a surgery to repair a detached or torn retina, viscous fluid 12 is preferably silicone oil, and viscous fluid 16 is preferably perfluorocarbon liquid. In addition, a saline solution 18 is typically present within

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posterior segment 13. Silicone oil 12 preferably has a viscosity of about 1000 to about 5000 centistokes. Perfluorocarbon liquid 16 preferably has a viscosity of about 6 to about 7 centistokes. Saline solution 18 preferably has a viscosity of about 1 centistoke. An exemplary silicone oil suitable for use as silicone oil 12 is the Silikon™ silicone oil 5 available from Alcon Laboratories, Inc. An exemplary perfluorocarbon liquid suitable for perfluorocarbon liquid 16 is Perfluoron® perfluorocarbon liquid sold by Alcon Laboratories, Inc. An exemplary saline solution suitable for saline solution 18 is BSS PLUS® intraocular irrigating solution sold by Alcon Laboratories, Inc.

Eye 14 has a cornea 20, a lens 22, a sclera 24, a choroid 26, a retina 28, and an 10 optic nerve 30. Cornea 20 and lens 22 generally define an anterior segment 32 of eye 14. Lens 22, choroid 26, and retina 28 generally define posterior segment 13 of eye 14. Retina 28 is physically attached to choroid 26 in a circumferential manner proximate pars plana 34.

As shown in FIG. 1, eye 14 has undergone a vitrectomy process in which the 15 vitreous humor has been cut and aspirated out of posterior segment 13, as described hereinabove. During this process, saline solution 18 was infused into eye 14 via an infusion cannula 62 to maintain the appropriate intraocular pressure. Also during this process, a detached portion or tear 36 of retina 28 was repositioned by injecting perfluorocarbon liquid 16 into posterior segment 13 via an injection cannula and syringe 20 (not shown) to cause detached portion or tear 36 to flatten against choroid 26 in the proper location. Once portion or tear 36 was properly located, a diathermy probe or a laser (not shown) was used to fuse portion or tear 36 in place. During this process, a conventional fiber optic light source 38 provided light for the surgeon, who viewed posterior segment 13 via a microscope. Light source 38 is inserted into posterior segment 13 via a 25 sclerotomy 39. Light source 38 is preferably operatively coupled to a port 40 of surgical system 10 via light fiber cabling 42.

As described hereinabove, perfluorocarbon liquid 16 is toxic when left in eye 14 for a period of weeks. Since detached portion or tear 36 of retina 28 requires a period of weeks to re-attach after the above-described surgical procedure, perfluorocarbon liquid 16 30 is only acceptable as a short-term tamponade to hold portion or tear 36 of retina 28 in the proper location against choroid 26. Therefore, perfluorocarbon liquid 16 is removed from eye 14 and replaced with silicone oil 12, a long-term tamponade.

Surgical system 10 includes a port 50 capable of providing proportional pressure to a microsurgical instrument connected thereto. For the preferred fluid/fluid exchange of the present invention, port 50 is fluidly coupled to an end 54 of a conventional syringe 56 via tubing 58. A second end 60 of syringe 56 is fluidly coupled to infusion cannula 62 via tubing 64. Tubing 58 and 64 are preferably conventional PVC tubing. Infusion cannula 62 is inserted into posterior segment 13 via a sclerotomy 66. Syringe 56 has a plunger 68 movably disposed within its hollow body 70.

Surgical system 10 also includes a port 52 capable of providing proportional vacuum to a microsurgical instrument attached thereto. Port 52 is preferably a part of conventional surgical cassette 72 that helps manage the aspiration flows of surgical system 10. U.S. Patent Nos. 4,493,695; 4,627,833 (Cook); 4,395,258 (Wang et al.); 4,713,051 (Steppe et al.); 4,798,850 (DeMeo et al.); 4,758,238; 4,790,816 (Sundblom et al.); 5,267,956; and 5,364,342 (Beuchat) all disclose tubeless or tube-type surgical cassettes and are incorporated herein in their entirety by reference. A collection bag 74 is fluidly coupled to surgical cassette 72.

For the preferred fluid/fluid exchange of the present invention, port 52 is fluidly coupled to an aspiration probe 76 having an extrusion cannula 77 via tubing 78. Tubing 78 is preferably conventional PVC tubing. Aspiration probe 76 and extrusion cannula 77 are inserted into posterior segment 13 via a sclerotomy 80.

FIG. 2 shows a block diagram of certain portions of the electronic and pneumatic sub-assemblies of surgical system 10. Surgical system 10 includes a regulated pneumatic pressure source 100 that is fluidly coupled to a proportional valve 102 via an input manifold 104. Pressure source 100 preferably supplies a constant source of pneumatic pressure on the order of about 85 psi. A suitable proportional valve for valve 102 is Model No. 002-AXXAVCAA sold by Porter Instrument Company, Inc. of Hatfield, Pennsylvania. Of course, other proportional valves may be used for valve 102. Proportional valve 102 is fluidly coupled to a solenoid valve 103 via a first valve output manifold 105. A vacuum pump or venturi 106 is fluidly coupled to solenoid valve 103 via a manifold 108. A suitable vacuum pump (venturi) for pump 106 is Model No. LX10 sold by PIAB of Hingham, Massachusetts. Of course, other pumps or venturis may be used for pump 106. Pump 106 has a vacuum manifold 110 that is fluidly coupled to a volume 72a of surgical cassette 72 and to port 52. Pump 106 also has an exhaust

manifold 112. In addition, proportional valve 102 is fluidly coupled to a solenoid valve 150 via a second valve output manifold 114. A reservoir 151 is fluidly coupled to solenoid valve 150 via a manifold 115. A manifold 116 fluidly couples reservoir 151 to port 50.

5 As is explained in more detail hereinbelow, a surgeon can switch the output of proportional valve 102 by opening and closing solenoid valves 103 and 150. When solenoid valve 103 is open and solenoid valve 150 is closed, proportional valve 102 supplies vacuum to port 52. When solenoid valve 150 is open and solenoid valve 103 is closed, proportional valve 102 supplies pneumatic pressure to port 50.

10 In surgical system 10, the surgeon chooses the desired vacuum or pressure level by manipulating a variable input device 120. Variable input device 120 is preferably a foot switch or foot pedal. Foot pedal 120 is operatively coupled to proportional valve 102 via conventional electronic cabling 122. A surgeon chooses the desired level of vacuum for port 52 or pressure for port 50 by manipulating foot pedal 120 to generate an input 15 signal 124 for proportional valve 102. More specifically, the surgeon can gradually open proportional valve 102 by depressing foot pedal 120 and can gradually close proportional valve 102 by “letting up” on foot pedal 120. The degree to which proportional valve 102 is open determines the pressure and air flow rate delivered to manifold 105 or manifold 114. The greater the air flow through proportional valve 102, the greater the vacuum 20 supplied to port 52, or the greater the pressure supplied to port 50. Although not shown in the block diagram of FIG. 2, a process control system is preferably operatively coupled to proportional valve 102, vacuum pump 106, vacuum manifold 110, second valve output manifold 114, and foot pedal 102 so as to give the surgeon precise control of the microsurgical instruments coupled to ports 50 or 52 of surgical system 10. The preferred 25 process control system is described in detail in U.S. Patent No. 5,674,194, which is commonly owned with the present invention and is incorporated herein in its entirety by reference.

FIG. 3 illustrates preferred embodiments of solenoid valve 150 and reservoir 151.

Tubing 152 supplies pneumatic pressure from second valve output manifold 114 to 30 solenoid valve 150, manifold 115, reservoir 151, manifold 116, and port or pneumatic



connector 50. Tubing 152 is preferably conventional PVC tubing. Tubing 152, solenoid valve 150, manifold 115, reservoir 151, and manifold 116 are preferably located within housing 11 of surgical system 10 generally behind port 50.

Although not shown in FIG. 3, reservoir 151 may also be located external to housing 11 of surgical system 10. For example, reservoir 151 may be fluidly coupled to tubing 58, as shown schematically in FIG. 1. As another example, syringe 56 may be modified from its conventional form to include reservoir 151 proximate its end 54. As a further example, the length and/or inner diameter of tubing 58 may be modified from its conventional form so as to incorporate the volume of reservoir 151.

FIG. 4 schematically illustrates a preferred embodiment of foot pedal 120 according to the present invention. Foot pedal 120 has a first position 200 corresponding to a fully undepressed position, a second position 202 corresponding to a fully depressed position, and a third position 204 corresponding to an about one-third depressed position. Position 204 is preferably indicated by a mechanical detent of foot pedal 120. Foot pedal 120 may be made by modifying the conventional foot pedal sold as part of the Accurus® surgical system mentioned hereinabove.

A conventional surgical system 10 is limited by the fact that it cannot supply pneumatic pressure to port 50 for the injection of viscous fluid 12 into eye 14 simultaneously with supplying vacuum to port 52 for the aspiration of viscous fluid 16 from eye 14. However, the addition of solenoid valve 150, reservoir 151, and manifolds 115 and 116 enable the delivery of a substantially constant pneumatic pressure to port 50 while proportional vacuum is also provided to port 52. Significantly, this ability allows the surgeon to minimize the potential of slippage of retina 28 and to maintain the intraocular pressure of eye 14 at a level very close to the desired intraocular pressure during the fluid/fluid exchange.

Referring again to FIGS. 1 and 2, a first volume V_1 may be defined by the volume of air within manifold 115, reservoir 151, manifold 116, tubing 58, and syringe 56 on the side of plunger 68 proximate tubing 58. A second volume V_2 may be defined by the volume of posterior segment 13 of eye 14 to be filled with silicone oil 12. As silicone oil 12 is injected into eye 14, syringe plunger 68 moves toward end 60 of syringe 56, increasing the volume of V_1 by the amount of oil injected. When all of the posterior segment 13 of eye 14 is filled with silicone oil 12, volume V_1 will have increased by an

amount V_2 . By using reservoir 151 to make volume V_1 substantially larger than volume V_2 , the silicone oil injection pressure can be maintained at a substantially constant pressure. More specifically, defining the initial silicone oil injection pressure in V_1 as P_1 and the post-injection pressure as P_2 with a volume of V_1+V_2 , Boyle's Law shows that P_1 5 will be approximately equal to P_2 if V_2 is small with respect to V_1 : $P_2 = P_1 \times (V_1 / (V_1 + V_2)) \Rightarrow P_2 \approx P_1$, if $V_1 \approx V_1 + V_2$ when $V_2 \ll V_1$.

At some point during the injection of silicone oil 12, the surgeon will also begin aspirating perfluorocarbon liquid 16 to counteract the rise in intraocular pressure caused by the injection of silicone oil 12. As is explained in more detail hereinbelow, when a 10 surgeon initiates aspiration of perfluorocarbon liquid 16 from posterior segment 13, solenoid valve 150 closes, eliminating the pneumatic pressure supplied from proportional valve 102, but isolating the silicone oil injection pressure in manifold 115, reservoir 151, manifold 116, tubing 58, and syringe 56. The isolated silicone oil injection pressure insures continued flow of silicone oil 12 into eye 14 via tubing 64.

FIG. 5 further illustrates how reservoir 151 functions to keep silicone oil injection pressure P_1 substantially constant during the injection of silicone oil 12. For one preferred embodiment of surgical system 10, tubing 58 and syringe 56 on the side of plunger 68 proximate tubing 58 have a volume V_0 of about twenty two (22) cubic centimeters, and reservoir 151 has a volume of about 12.5 cubic centimeters. For a typical adult human 15 eye, the volume V_2 of posterior segment 13 to be filled with silicone oil 12 is about 5 cubic centimeters. When V_0 was increased by V_2 , as would occur during the injection of 20 5 cubic centimeters of silicone oil, an injection pressure P_0 of about 40 psi decreased about 7 psig (about 17.5 percent). In contrast, with a reservoir 151 having a volume of 12.5 cubic centimeters added to V_0 for a total volume V_1 of about 34.5 cubic centimeters, an injection pressure P_1 of about 40 psi decreased only about 4.8 psig (about 12 percent) when V_1 was increased by V_2 . As another example, an injection pressure P_0 of about 80 25 psi decreased about 14 psig (about 17.5 percent) when V_0 was increased by V_2 . In contrast, with a reservoir 151 having a volume of 12.5 cubic centimeters added to V_0 for a total volume V_1 of about 34.5 cubic centimeters, an injection pressure P_1 of about 80 psi decreased only about 9.8 psig (about 12 percent) when V_1 was increased by V_2 . Similar 30 variances of P_1 were observed for injection pressures of 50 psi, 60 psi, and 70 psi, as shown in FIG. 5. Boyle's Law shows that the variance of P_1 may be reduced below 12

percent by increasing the volume of reservoir 151, if desired, for specific surgical systems 10. For example, this variance of P_1 may be reduced to 10 percent, 8 percent, 6 percent, 4 percent, 2 percent, or below.

Referring to FIGS. 1 through 5, the preferred method of operating foot pedal 120 according to the present invention so as to perform a fluid/fluid exchange of perfluorocarbon liquid 16 and silicone oil 12 is described in greater detail. When foot pedal 120 is in position 200, proportional valve 102 does not supply pneumatic pressure or vacuum to ports 50 or 52, respectively. Solenoid valve 103 is in the closed position, and solenoid valve 150 is in the open position. Silicone oil 12 is not being injected into posterior segment 13 via infusion cannula 62, and perfluorocarbon liquid 16 is not being aspirated via aspiration probe 76.

When a surgeon gradually moves foot pedal 120 from position 200 to position 204, pneumatic pressure is supplied to manifold 115, reservoir 151, manifold 116, port 50, tubing 58, and syringe 56 in gradually increasing amounts. This is accomplished via a change in electrical signal 124 from foot pedal 120 to proportional valve 102 communicated via electrical cabling 122. The minimum pneumatic pressure is preferably 0 psi (position 200), and the maximum pneumatic pressure is preferably about 80 psi (position 204). Such proportional pneumatic pressure causes silicone oil 12 from syringe 56 and tubing 64 to be injected into posterior segment 13 via infusion cannula 62. During this process, a clamping mechanism (not shown) within surgical cassette 72 is preferably in the closed position to prevent passive flow of perfluorocarbon liquid 16 into surgical cassette 72. Therefore, the intraocular pressure of eye 14 gradually begins to rise.

If the surgeon applies additional downward force to foot pedal 120 at position 204, he or she overcomes a mechanical detent in foot pedal 120. While overcoming this detent, the printed circuit board electronics of surgical system 10 close solenoid valve 150 and open solenoid valve 103, fluidly coupling vacuum pump 106 to first valve output manifold 105. Closure of solenoid valve 150 causes the injection pressure P_1 in manifold 115, reservoir 151, manifold 116, port 50, tubing 58, and syringe 56 to be maintained, resulting in the continued flow of silicone oil into eye 14 via tubing 64. Furthermore, the printed circuit board electronics of surgical system 10 actuate the clamping mechanism within surgical cassette 72 to an open position allowing flow of perfluorocarbon liquid 16 from tubing 78 into cassette 72.

When a surgeon gradually moves foot pedal 120 from position 204 to position 202, vacuum is supplied to port 52, tubing 78, aspiration probe 76, and extrusion cannula 77 in increasing amounts. This is accomplished via a change in electrical signal 124 from foot pedal 120 to proportional valve 102 communicated via electrical cabling 122. The 5 minimum vacuum is preferably 0 mmHg (position 204), and the maximum vacuum is preferably about 600 mmHg (position 202). Such proportional vacuum causes perfluorocarbon liquid 16 to be aspirated from posterior segment 13 into cassette 72 and collection bag 74. This vacuum counteracts the rise in intraocular pressure caused by the injection of silicone oil 12.

10 As the intraocular pressure begins to decrease due to aspiration of perfluorocarbon liquid 16, the surgeon lets up on foot pedal 120, controlling the flow of aspirated perfluorocarbon liquid 16 to more closely match the injection flow rate of silicone oil 12. In this manner, the surgeon quickly brings the intraocular pressure to its desired level.

15 During this replacement of perfluorocarbon liquid 16 with silicone oil 12, the surgeon visually monitors eye 14 to prevent the intraocular pressure from rising to a dangerously high level (a "hard eye" condition) or to a dangerously low level (a "soft eye" condition). Significantly, because of the added volume of reservoir 151 and solenoid valve 150, the silicone oil injection pressure P_1 remains substantially constant during the aspiration of perfluorocarbon liquid 16. This, combined with the design of foot pedal 20 120, allows the surgeon to more effectively control the intraocular pressure of eye 14, minimizing risk to the patient.

25 From the above, it may be appreciated that the present invention provides improved apparatus and methods for tamponading a retinal tear or detachment. The present invention minimizes retinal slippage and variations in intraocular pressure during a fluid/fluid exchange. The present invention also provides the surgeon with an easier method of controlling a fluid/fluid exchange.

The present invention is illustrated herein by example, and various modifications 30 may be made by a person of ordinary skill in the art. For example, although the preferred apparatus and methods are described hereinabove in connection with a fluid/fluid exchange of perfluorocarbon liquid and silicone oil in vitreoretinal surgery, the present invention is applicable to the simultaneous injection and aspiration of other viscous fluids.

As another example, the present invention is also applicable to other types of surgeries other than vitreoretinal surgery.

It is believed that the operation and construction of the present invention will be apparent from the foregoing description. While the apparatus and methods shown or described above have been characterized as being preferred, various changes and modifications may be made therein without departing from the spirit and scope of the invention as defined in the following claims.

THE CLAIMS DEFINING THE INVENTION ARE AS FOLLOWS:

1. A method of injecting a first retinal tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment, including the steps of:
 - providing a surgical system capable of supplying pneumatic pressure and vacuum;
 - injecting said first retinal tamponading fluid into said posterior segment using pneumatic pressure from said system;
 - changing a mode of operation of said system to provide vacuum and pneumatic pressure; and
 - aspirating said second retinal tamponading fluid from said posterior segment using vacuum from said system, wherein said pneumatic pressure remains substantially constant during said aspirating step.
2. The method of claim 1 wherein said eye is a human eye.
3. The method of claim 1 wherein said pneumatic pressure exhibits a decrease of about twelve percent or less during said aspirating step.
4. The method of claim 1 wherein said first retinal tamponading fluid is a silicon oil, and said second retinal tamponading fluid is a perfluorocarbon liquid.
5. A surgical system for injecting a first retinal tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment, said posterior segment having a volume, including:
 - an assembly capable of supplying pneumatic pressure and vacuum;
 - a syringe; and
 - tubing fluidly coupling said syringe to said assembly;

wherein a first volume of air in said tubing and said syringe is greater than said volume of said posterior segment.
6. The surgical system of claim 5 further including:
 - an infusion cannula fluidly coupled to said syringe;
 - an aspiration probe fluidly coupled to said assembly; and
 - an extrusion cannula coupled to said aspiration probe.
7. The surgical system of claim 6 wherein said infusion cannula and said extrusion cannula are for insertion into said posterior segment.



8. The surgical system of claim 5 wherein said eye is a human eye.

9. The surgical system of claim 5 wherein said first retinal tamponading fluid is a silicon oil, and said second retinal tamponading fluid is a perfluorocarbon liquid.

10. The surgical system of claim 5 further including a housing and wherein:
5 said assembly is disposed within said housing and includes a reservoir fluidly coupled with said tubing and said syringe;

 said tubing and said syringe are disposed outside of said housing; and
 said first volume includes a volume of air in said reservoir, said tubing, and said
 syringe.

10 11. The surgical system of claim 10 wherein:
 said assembly includes:

 a regulated pressure source;
 a proportional valve fluidly coupled to said regulated pressure source; and
 a vacuum pump fluidly coupled to said proportional valve; and

15 said reservoir is fluidly coupled to said proportional valve.

12. A surgical system for injecting a first viscous fluid into a target tissue simultaneous with aspirating a second viscous fluid from said target tissue, including:
 an assembly capable of supplying pneumatic pressure and vacuum to at least one
 microsurgical instrument;

20 a foot pedal, operatively coupled to said assembly, including:
 a first range of motion in a generally vertical plane in which said assembly
 supplies proportional pneumatic pressure; and
 a second range of motion in a generally vertical plane in which said
 assembly supplies a substantially constant pneumatic pressure and proportional
 vacuum.

25 13. The surgical system of claim 12 wherein said foot pedal includes a
 mechanical detent separating said first range of motion and said second range of motion.

14. The surgical system of claim 12 wherein said first range of motion
 includes about one third of a full range of motion in a generally vertical plane of said foot
30 pedal.



15. The surgical system of claim 13 wherein said first range of motion is from a first position corresponding to a fully undepressed position, to a second position corresponding to said mechanical detent.

16. The surgical system of claim 15 wherein said second range of motion is 5 from said second position to a third position corresponding to a fully depressed position.

17. The surgical system of claim 16 wherein moving said foot pedal in said first range of motion toward said second position increases an amount of pneumatic pressure supplied by said assembly.

18. The surgical system of claim 16 wherein moving said foot pedal in said 10 second range of motion toward said third position increases an amount of vacuum supplied by said assembly.

19. The surgical system of claim 12 wherein said target tissue is a human eye.

20. The surgical system of claim 12 wherein said target tissue is a posterior segment of a human eye.

15 21. The surgical system of claim 20 wherein said first viscous fluid is a first retinal tamponading fluid, and said second viscous fluid is a second retinal tamponading fluid.

22. The surgical system of claim 21 wherein said first retinal tamponading fluid is a silicon oil, and said second retinal tamponading fluid is a perfluorocarbon liquid.

20 23. The surgical system of claim 12 wherein said at least one microsurgical instrument includes:

an infusion cannula and a syringe for injecting said first viscous fluid into said target tissue; and

25 an aspiration probe and an extrusion cannula for aspirating said second viscous fluid from said target tissue.

24. The surgical system of claim 12 wherein said substantially constant pneumatic pressure includes a pneumatic pressure decrease of about twelve percent or less.

30 25. A surgical system for injecting a first retinal tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment, said posterior segment having a volume, including:



a single pneumatic assembly capable of supplying pneumatic pressure and vacuum, said assembly including a reservoir;

a syringe having:

a hollow bore with a first end and a second end; and

5 a plunger movably disposed in said hollow bore between said first end and said second end; and

tubing fluidly coupling said first end of said hollow bore to said reservoir;

wherein a volume of said reservoir, said tubing, and said hollow bore on a side of said plunger proximate said first end is greater than said volume of said posterior

10 segment.

26. The surgical system of claim 25 further including a housing and wherein:

said assembly is disposed within said housing; and

said tubing and said syringe are disposed outside of said housing.

27. The surgical system of claim 26 wherein:

15 said assembly includes:

a regulated pressure source;

a proportional valve fluidly coupled to said regulated pressure source; and

a vacuum pump fluidly coupled to said proportional valve; and

said reservoir is fluidly coupled to said proportional valve.

20 28. The surgical system of claim 25 wherein said first retinal tamponading fluid is a silicon oil, and said second retinal tamponading fluid is a perfluorocarbon liquid.

29. A method of injecting a first tamponading fluid into a posterior segment of an eye simultaneous with aspirating a second retinal tamponading fluid from said posterior segment substantially as herein described with reference to the accompanying 25 drawings.

30 30. A surgical system substantially as herein described with reference to the accompanying drawings.

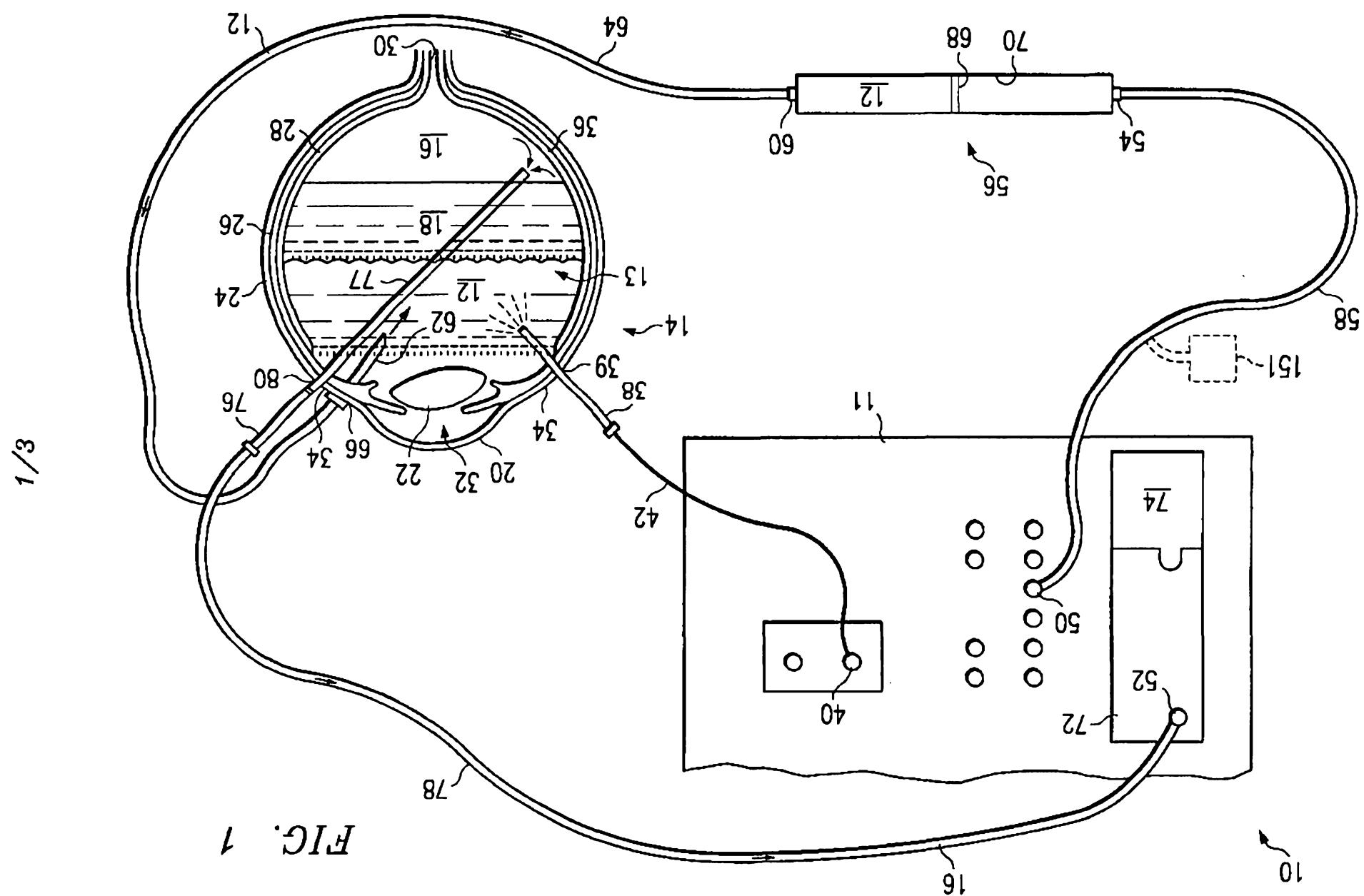
DATED: 3 September, 2002

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ALCON LABORATORIES, INC..





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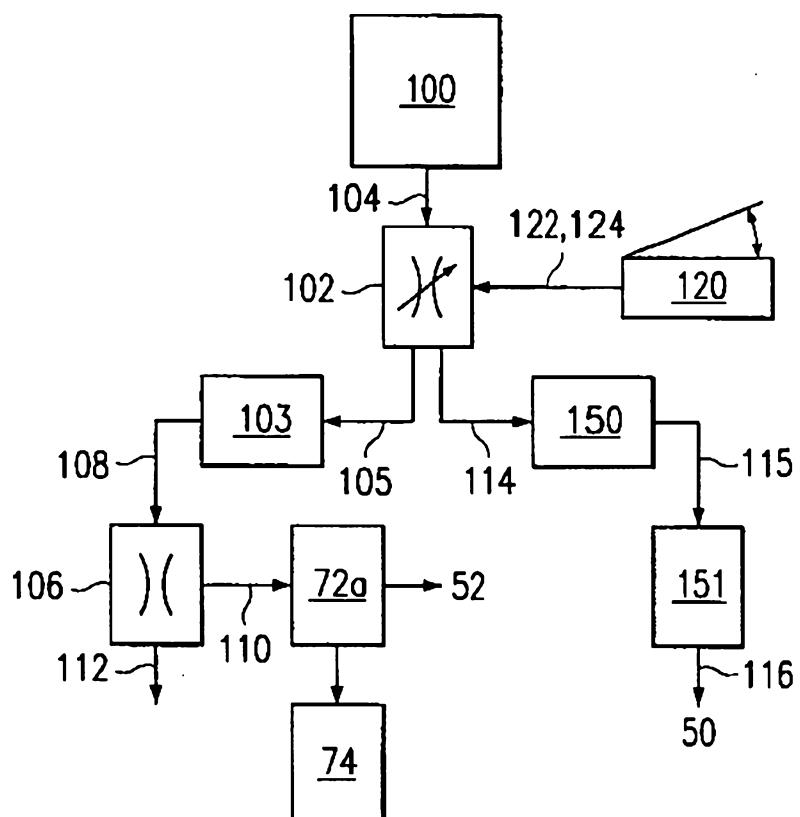


FIG. 2

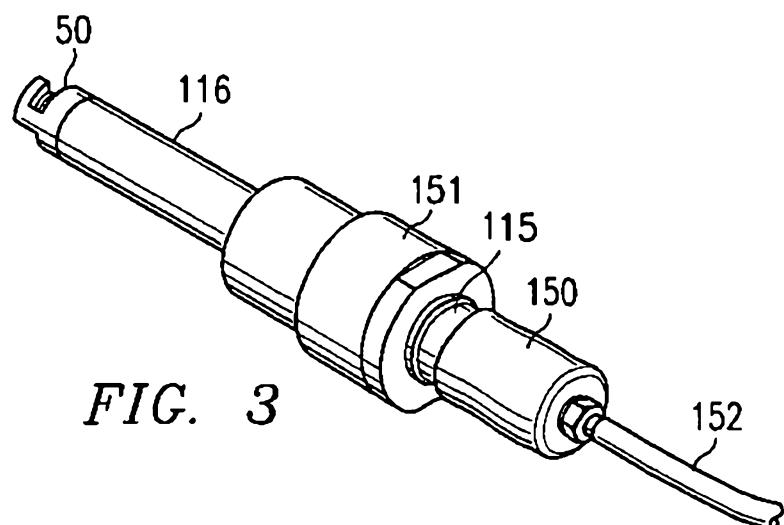


FIG. 3

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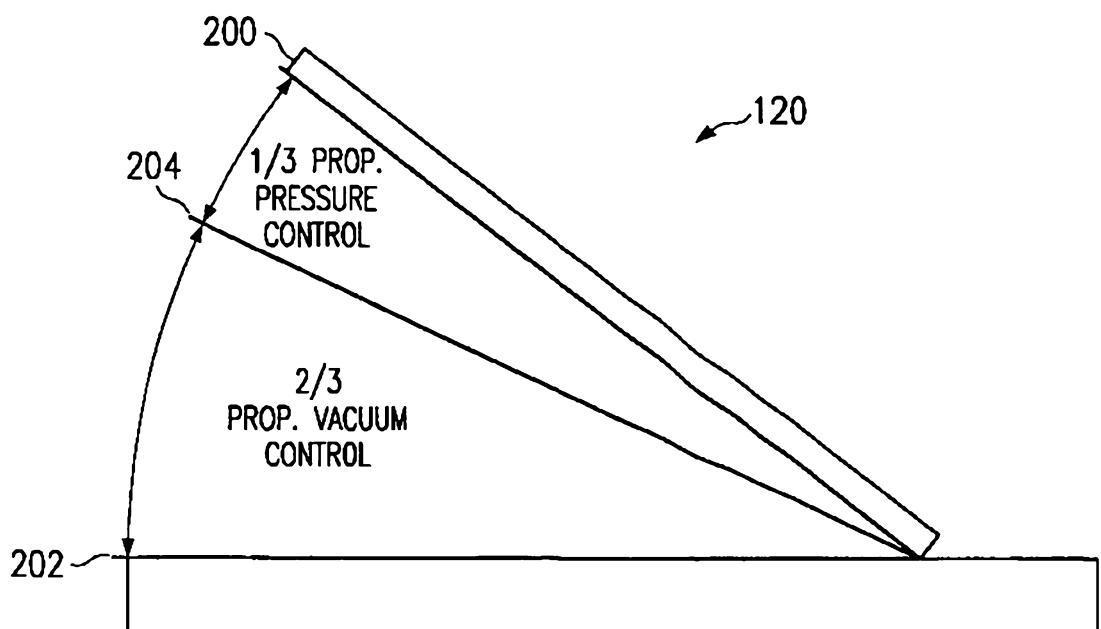


FIG. 4

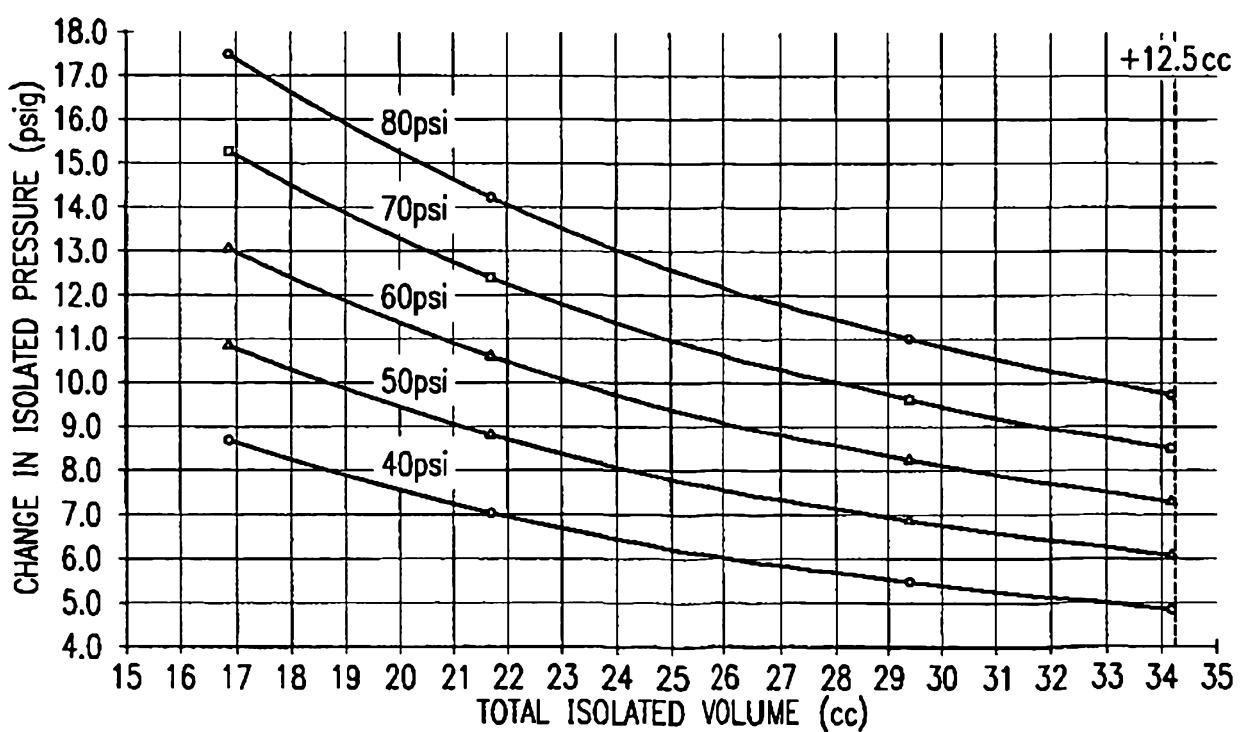


FIG. 5