



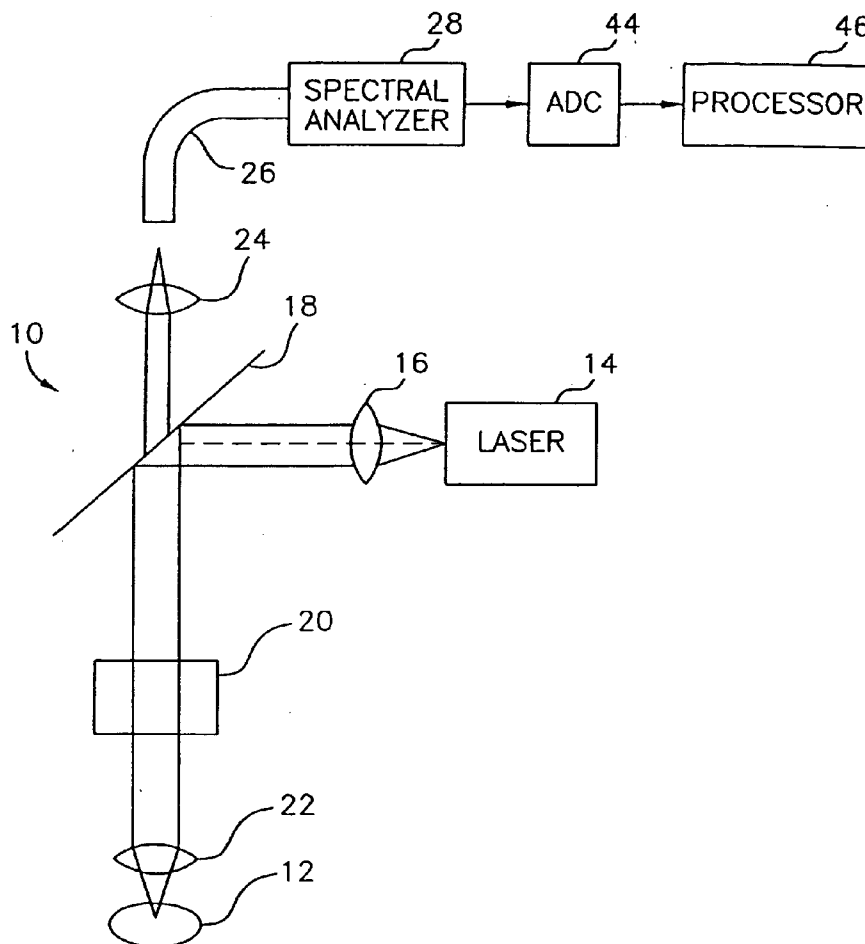
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(19) **United States**(12) **Patent Application Publication**  
**Bearman et al.**(10) **Pub. No.: US 2009/0095919 A1**(43) **Pub. Date: Apr. 16, 2009**(54) **SYSTEM AND METHOD FOR MONITORING  
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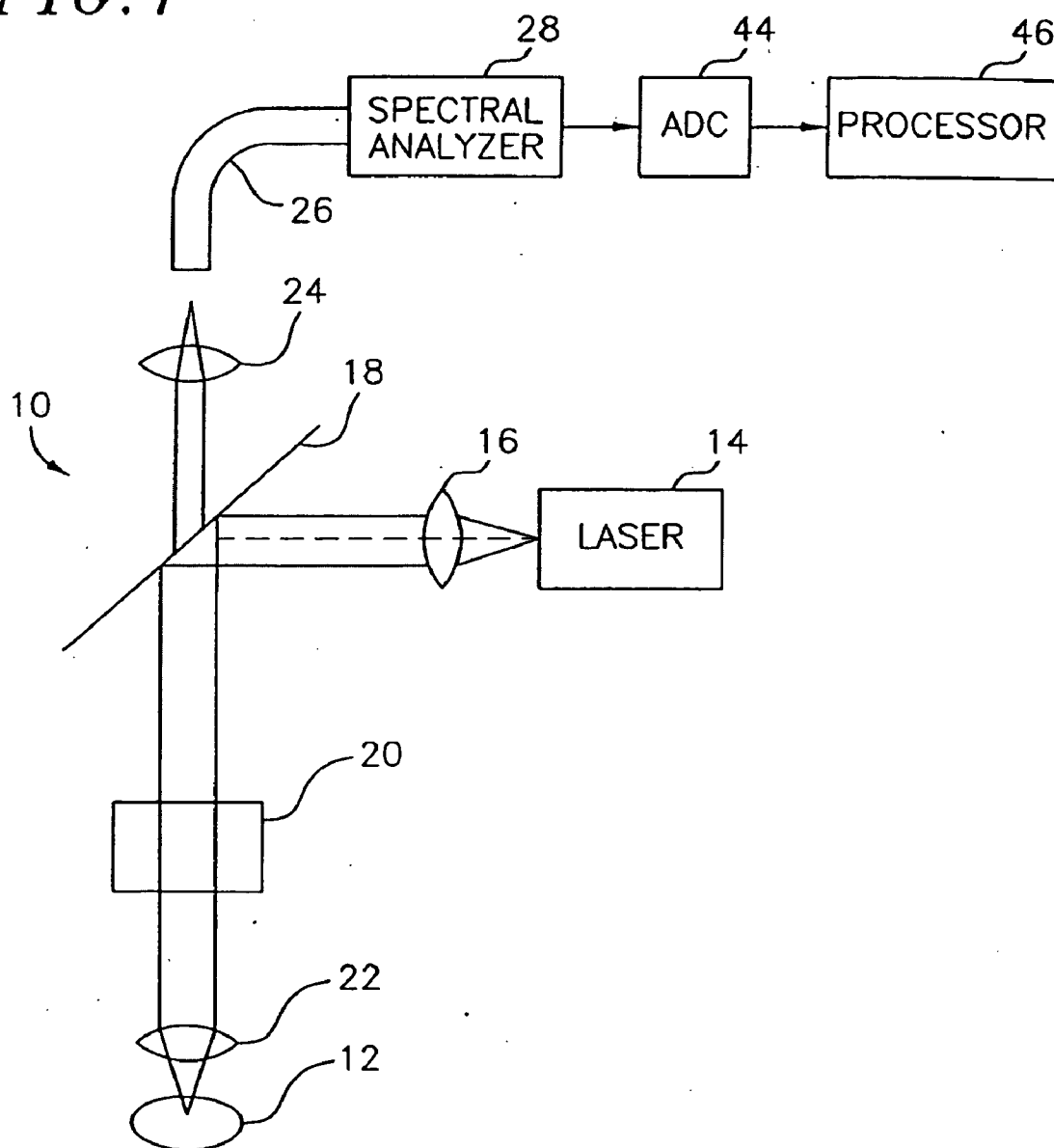
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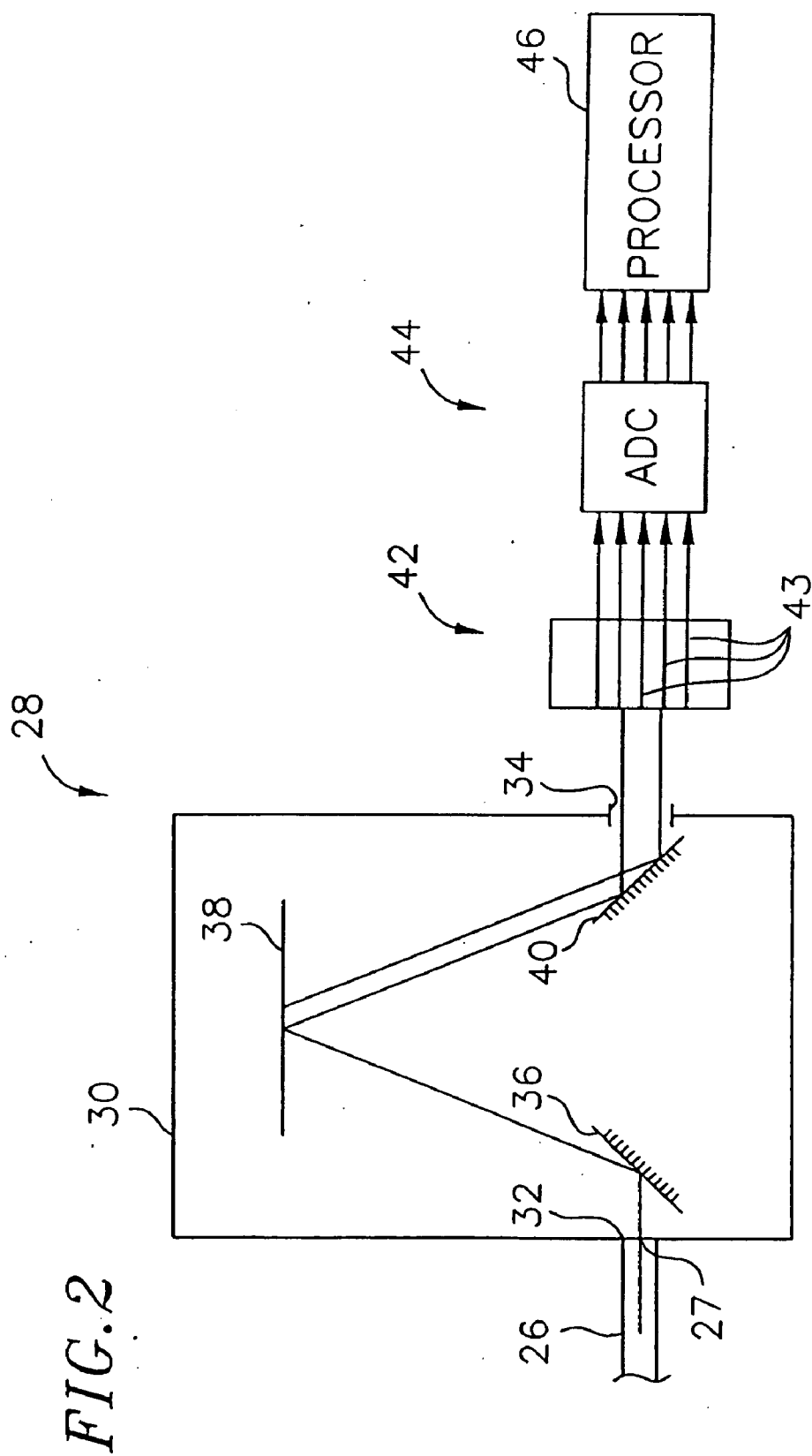
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**PASADENA, CA 91109-7068 (US)**(21) Appl. No.: **12/335,380**(22) Filed: **Dec. 15, 2008****Related U.S. Application Data**(63) Continuation of application No. 10/817,297, filed on  
Apr. 2, 2004, which is a continuation of application  
No. 10/159,703, filed on May 28, 2002, now Pat. No.6,750,036, which is a continuation of application No.  
09/628,219, filed on Jul. 28, 2000, now Pat. No. 6,403,  
332.(60) Provisional application No. 60/146,490, filed on Jul.  
30, 1999, provisional application No. 60/164,504,  
filed on Nov. 9, 1999.**Publication Classification**(51) **Int. Cl.**  
**G01N 21/64** (2006.01)(52) **U.S. Cl.** ..... **250/459.1**(57) **ABSTRACT**

A system and method for monitoring cellular activity in a cellular specimen. According to one embodiment, a plurality of excitable markers are applied to the specimen. A multi-photon laser microscope is provided to excite a region of the specimen and cause fluorescence to be radiated from the region. The radiating fluorescence is processed by a spectral analyzer to separate the fluorescence into respective wavelength bands. The respective bands of fluorescence are then collected by an array of detectors, with each detector receiving a corresponding one of the wavelength bands.

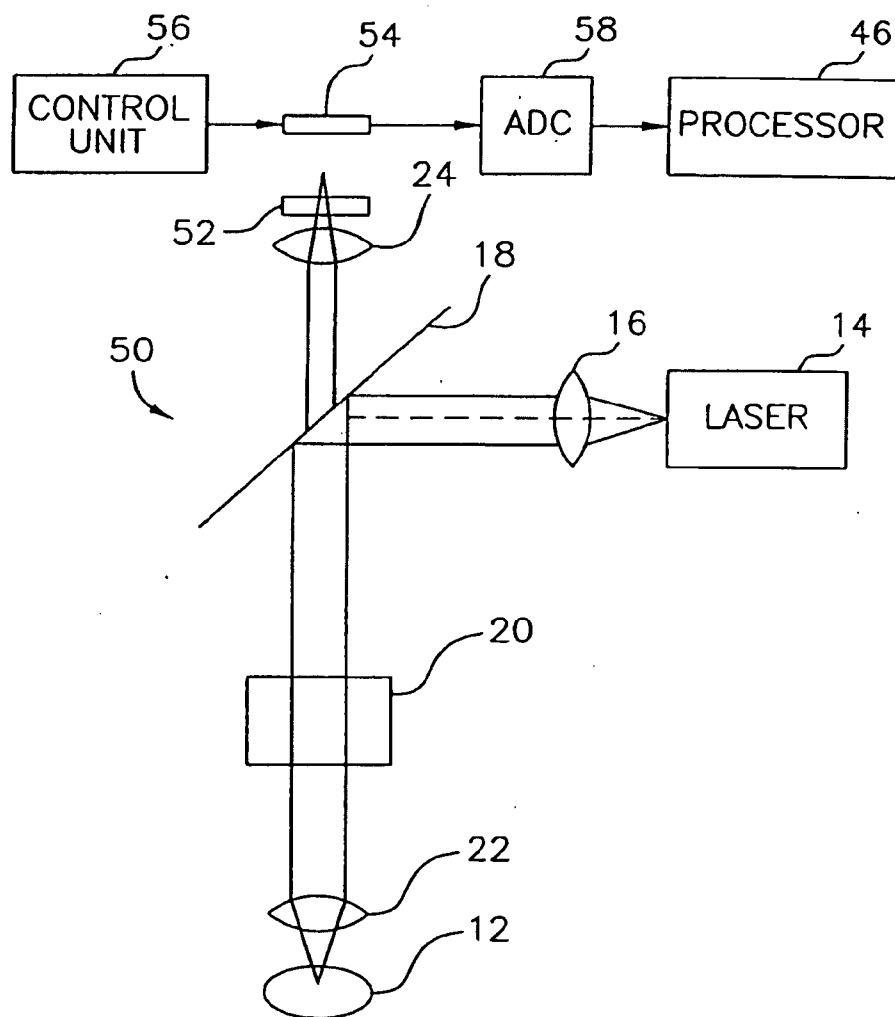


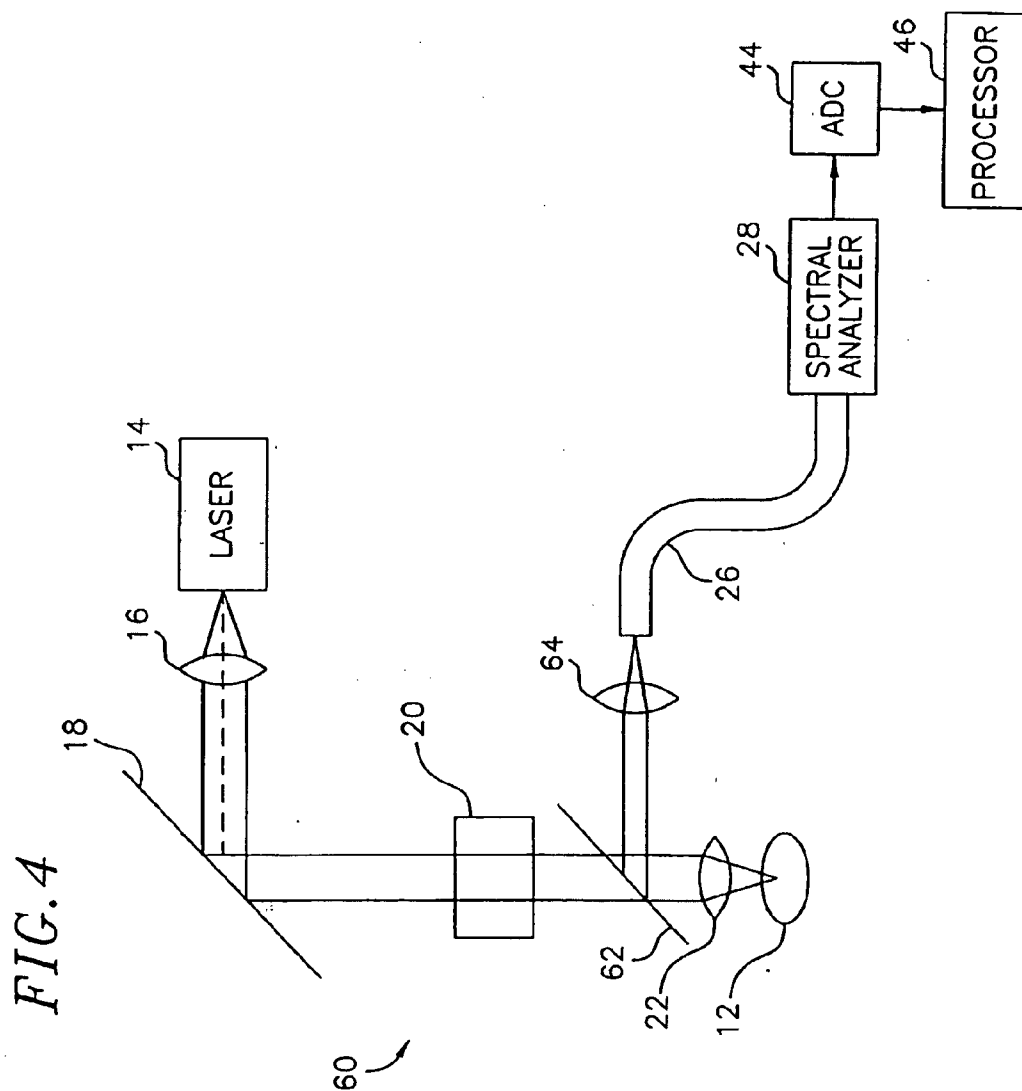
*FIG. 1*

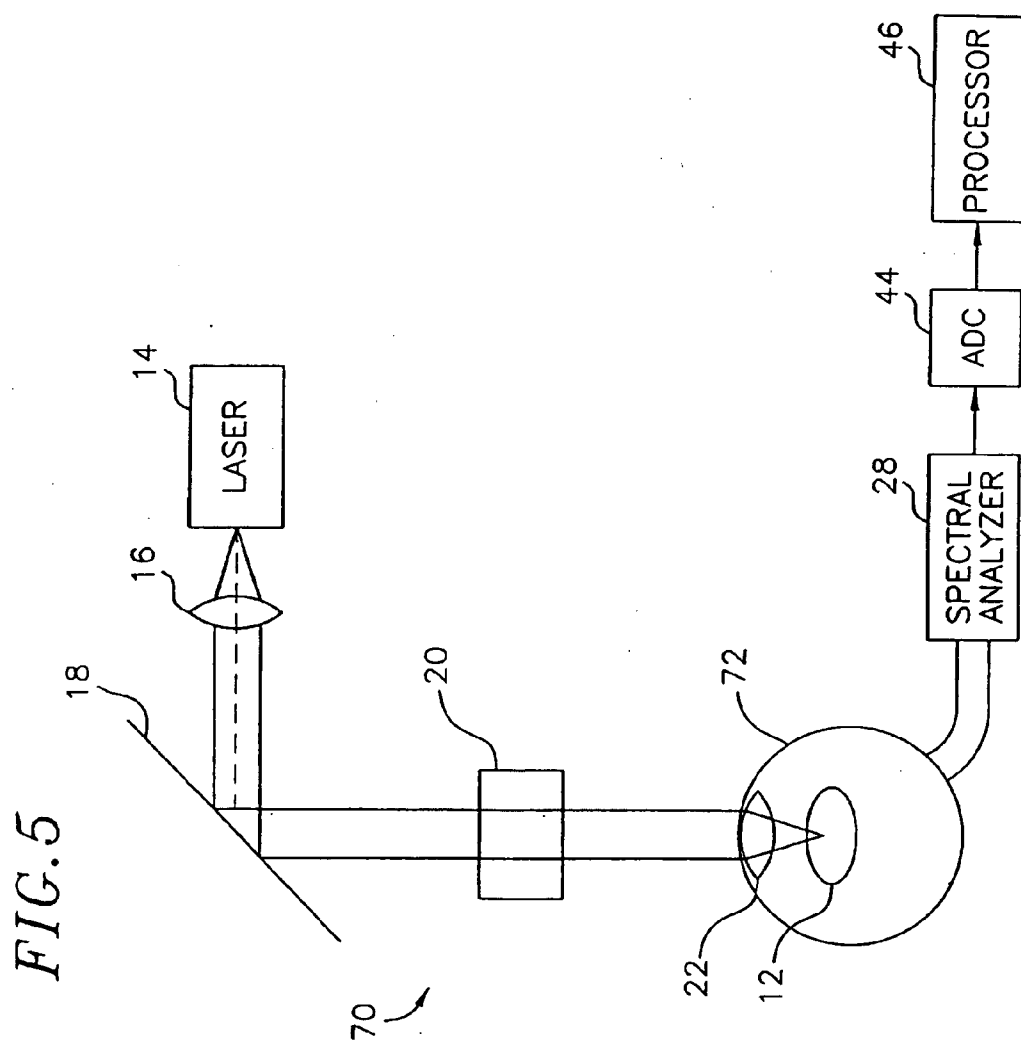


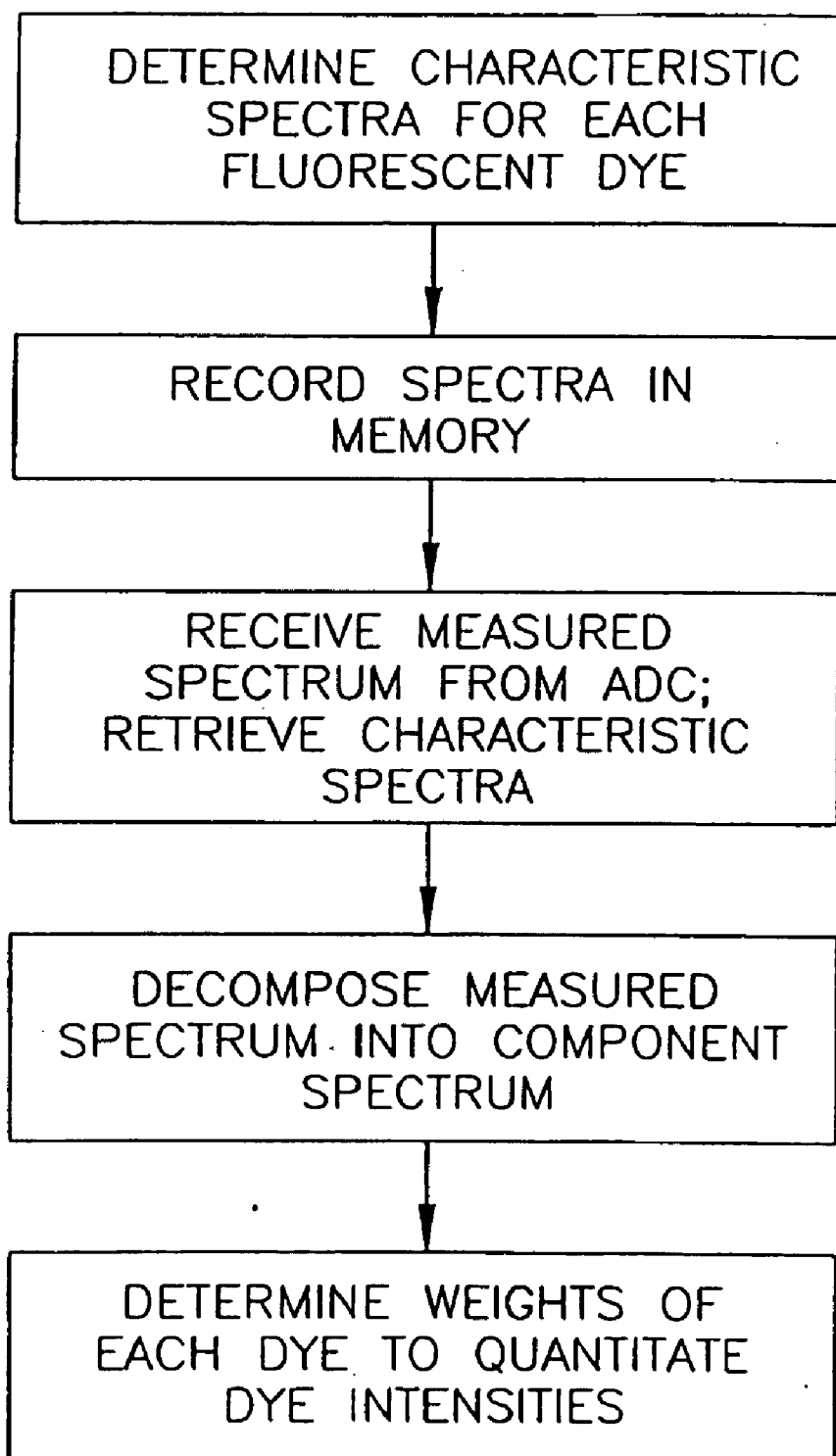


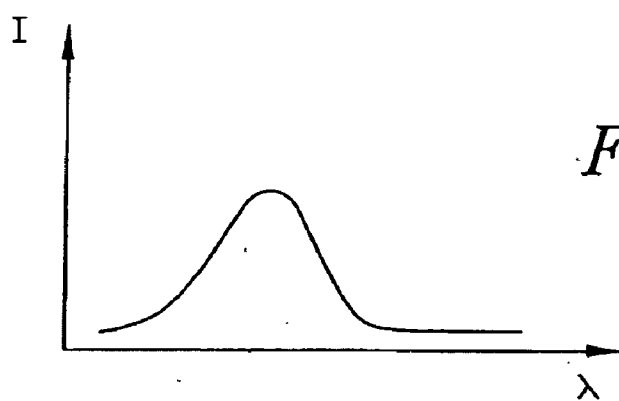
*FIG. 3*



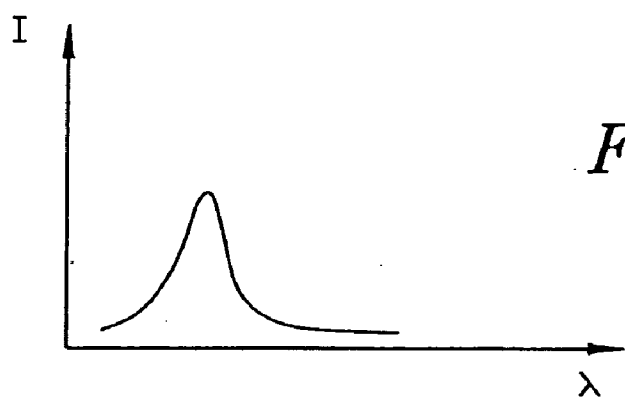




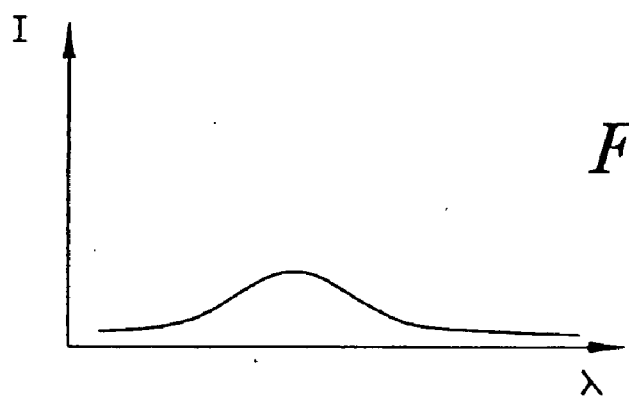
*FIG. 6*



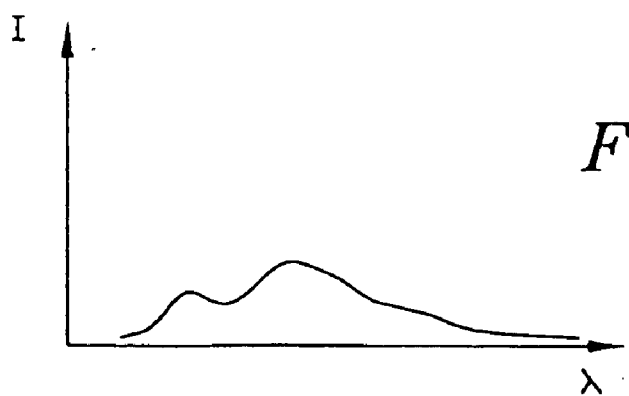
*FIG. 7a*



*FIG. 7b*



*FIG. 7c*



*FIG. 7d*



## SYSTEM AND METHOD FOR MONITORING CELLULAR ACTIVITY

### CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] The present application is a continuation of U.S. application Ser. No. 10/817,297, filed Apr. 2, 2004, which is a continuation of U.S. application Ser. No. 10/159,703, filed May 28, 2002, which is a continuation of U.S. application Ser. No. 09/628,219, filed Jul. 28, 2000, which issued as U.S. Pat. No. 6,403,332, on Jun. 11, 2002, which claims priority to U.S. Provisional Application Nos. 60/146,490, filed Jul. 30, 1999 and 60/164,504, filed Nov. 9, 1999, the disclosures of which are incorporated herein by reference.

### FIELD OF THE INVENTION

[0002] The present invention relates to the monitoring of cellular activity through the use of excitable markers. More particularly, the invention relates to a system and method for using a plurality of fluorescent probes to monitor cellular activity.

### BACKGROUND OF THE INVENTION

[0003] Presently, fluorescence microscopy is one of the most widely used microscopy techniques, as it enables the molecular composition of the structures being observed to be identified through the use of fluorescently-labeled probes of high chemical specificity, such as antibodies. However, its use is mainly confined to studies of fixed specimens because of the difficulties of introducing antibody complexes into living specimens. For proteins that can be extracted and purified in reasonable abundance, these difficulties can be circumvented by directly conjugating a fluorophore to a protein and introducing this back into a cell. It is believed that the fluorescent analogue behaves like the native protein and can therefore serve to reveal the distribution and behavior of this protein in the cell.

[0004] An exciting, new development in the use of fluorescent probes for biological studies has been the development of the use of naturally fluorescent proteins as fluorescent probes, such as green fluorescent protein (GFP). The gene for this protein has been cloned and can be transfected into other organisms. This can provide a very powerful tool for localizing regions in which a particular gene is expressed in an organism, or in identifying the location of a particular protein. The beauty of the GFP technique is that living, unstained samples can be observed. There are presently several variants of GFP which provide spectrally distinct emission colors.

[0005] Conventionally, fluorescence microscopy only worked well with very thin specimens or when a thick specimen was cut into sections, because structures above and below the plane of focus gave rise to interference in the form of out-of-focus flare. However, this can be overcome by optical sectioning techniques, such as multi-photon fluorescence microscopy.

[0006] Multi-photon fluorescence microscopy involves the illumination of a sample with a wavelength around twice the wavelength of the absorption peak of the fluorophore being used. For example, in the case of fluorescein which has an absorption peak around 500 nm, 1000 nm excitation could be used. Essentially no excitation of the fluorophore will occur at this wavelength. However, if a high peak-power, pulsed laser is used (so that the mean power levels are moderate and do not damage the specimen), two-photon events will occur at the point of focus. At this point the photon density is sufficiently high that two photons can be absorbed by the fluorophore

essentially simultaneously. This is equivalent to a single photon with an energy equal to the sum of the two that are absorbed. In this way, fluorophore excitation will only occur at the point of focus (where it is needed) thereby eliminating excitation of the out-of-focus fluorophore and achieving optical sectioning.

[0007] Often, multiple fluorophores are used, with each fluorophore having a different spectra, some of which may overlap. Typically, the ability to distinguish between the respective fluorophores is only possible where the excitation spectra are separated, or where the fluorescence lifetimes are distinct.

[0008] Another approach is to selectively excite different fluorophores by using various excitation photon wavelengths, each of which will approximate the wavelength of the absorption peak of a corresponding fluorophore. Such an approach is not practical for a number of reasons. Firstly, it is difficult to rapidly tune the excitation wavelength of the laser providing the excitation photons. Secondly, there is typically a very broad excitation spectrum, so that such an approach requires a significant amount of time.

[0009] Thus, the need exists for a system and method for efficiently monitoring a plurality of fluorescent probes, and to record emissions spectra relating to those probes for subsequent analysis. The present invention addresses these needs.

### SUMMARY OF THE INVENTION

[0010] Briefly, the present invention is directed to a system and method for monitoring cellular activity in a cellular specimen. According to one illustrative embodiment of the invention, a plurality of excitable markers are applied to the specimen. A multi-photon laser microscope is provided to excite a region of the specimen and cause fluorescence to be radiated from the region. The radiating fluorescence is processed by a spectral analyzer to separate the fluorescence into wavelength bands. The respective fluorescence bands are then collected by an array of detectors, with each detector receiving a corresponding one of the wavelength bands.

[0011] According to another embodiment, the invention is directed to a system for monitoring cellular activity in a cellular specimen that contains a plurality of excitable markers. The system includes a laser microscope that is operative to excite the markers in a region of the specimen, so that those markers in the region radiate fluorescence. The system also includes a tunable filter that is operative to process the fluorescence and to pass a portion of the fluorescence wavelengths radiated by the markers. The system still further includes a detector that is operative to receive the processed fluorescence wavelengths.

[0012] In still another embodiment, the invention is directed to a system for monitoring cellular activity, including a two-photon laser microscope that is operative to excite the markers in a region of the specimen such that the markers in the region radiate fluorescence. The system also includes a detector that is operative to receive non-descanned fluorescence from the specimen.

### BRIEF DESCRIPTION OF THE DRAWINGS

[0013] These and other features and advantages of the present invention will be better understood by reference to the following detailed description when considered conjunction with the accompanying drawings wherein:

[0014] FIG. 1 is a schematic diagram of a first illustrative embodiment of the present invention;

[0015] FIG. 2 is a schematic diagram that illustrates one embodiment of a spectral analyzer included in the system of FIG. 1;

[0016] FIG. 3 is a schematic diagram that illustrates a system according to another illustrative embodiment of the invention;

[0017] FIG. 4 is a schematic diagram that illustrates yet another illustrative embodiment of the invention;

[0018] FIG. 5 is a schematic diagram that illustrates still another embodiment of the invention;

[0019] FIG. 6 is a flow chart that depicts the operational flow of processing software to process spectral data received by the systems of any of FIGS. 1 through 5 according to one illustrative embodiment of the invention;

[0020] FIGS. 7a-c depict emissions spectra for various fluorescent dyes; and

[0021] FIG. 7d depicts a measured spectrum from a specimen that contains plural different dyes.

#### DETAILED DESCRIPTION OF THE INVENTION

[0022] Referring to FIG. 1, a novel system 10 is disclosed for capturing spectral data from a specimen 12 to which a plurality of excitable markers have been applied. In one embodiment, at least two fluorescent dyes (i.e., fluorescent probes) are applied to the specimen. The fluorescent dyes have respective emission spectra that may or may not overlap. In the case where the emission spectra are very similar, it becomes difficult to separate out the emission spectra to determine the contributions of each of the fluorescent dyes to the observed spectra. System 10 facilitates making such determinations in an efficient, reliable manner.

[0023] As shown in FIG. 1, system 10 includes a laser 14 that generates laser light. The light emitted by laser 14 is focused by a lens 16 onto a short pass dichroic mirror 18. As is well known, the dichroic mirror 18 selectively reflects light according to its wavelength. Thus, the dichroic mirror is selected such that it reflects the light emitted by laser 14.

[0024] The reflected light from dichroic mirror 18 is directed toward scanning optics, shown schematically at 20. The scanning optics may include a controllable deflection unit, or any other suitable structure that allows the reflected light to be redirected for scanning of the specimen 12 by the laser light, as is well known to those skilled in the art.

[0025] The directed light from scanning optics 20 is imaged by a microscope lens 22 onto or into the specimen 12. The laser light excites the fluorescent dyes in the region where the light is directed, such that those dyes fluoresce and emit light having respective emissions spectra.

[0026] In one embodiment, laser 14 is a two-photon laser. As is well known, a two-photon laser microscope depends on the two-photon effect, by which the fluorescent dyes are excited not by a single photon, but rather by two relatively low energy photons that are absorbed contemporaneously by a fluorescent dye. Thus, the requirement for two coincident (or near coincident) photons to achieve excitation of the fluorescent dye means that only focused light reaches the required intensities and that scattered light does not cause excitation of the fluorescent dyes. As such, a two-photon laser microscope is inherently insensitive to the effects of light scattering in thick slices. Alternatively, the laser 14 may comprise some other multi-photon laser, or a single-photon laser.

[0027] The fluorescence radiated by the excited dyes is focused by the microscope lens 22, and passes through the scanning optics 20 and dichroic mirror 18. The fluorescence is then focused by a lens 24 and directed to a light guide 26 that delivers the focused light to a spectral analyzer 28. Spectral analyzer 28 receives the light and disperses the light into

respective wavelength bands. Each band is detected by a corresponding detector, and the intensity of each band is recorded and processed to determine the ingredients of the received fluorescence, as is described in more detail below in connection with FIG. 2.

[0028] Referring to FIG. 2, there is shown one illustrative embodiment of spectral analyzer 28. Spectral analyzer 28 includes a housing 30 formed with a light entrance opening 32 and a light exit opening 34. Light entrance opening 32 is connected to light guide 26 to receive light from the light guide. Preferably, the distal end of light guide 26 includes an exit slit 27 to permit the delivery of fluorescence from light guide 26 to spectral analyzer 28. Mounted within spectral analyzer 28 is a first mirror 36 that directs the incoming light to a grating 38, which disperses the light over appropriate wavelength range. The dispersed light is then directed to a second mirror 40 that directs the dispersed light through the exit opening 34. In place of the grating 38, spectral analyzer 28 may alternatively include a prism or other light-dispersing structure.

[0029] Aligned with exit opening 34 is a detector array 42 consisting of individual detectors 43. The detector array 42 may take many different forms, such as an array of photomultiplier tubes (PMTs), multiple window PMTs, position-dependant wire detectors, position/time-sensitive detectors, a photodiode array, an intensified photodiode array, charge-coupled devices (CCDs), intensified CCDs, an SIT or other video camera, or any other suitable optical-to-electrical transducer.

[0030] In any event, the detector array 42 is preferably a linear array, with the respective wavelength bands being incident upon a corresponding one of the detectors 43. Each detector 43 in the array receives the light incident upon it and generates a corresponding analog electrical signal. The electrical signals are then introduced to respective analog-to-digital converters (shown schematically at 44) which convert the incoming analog signals into corresponding digital signals. The digital signals are then delivered to a processor 46 that processes the digital signals to determine the constituents of the emissions spectra, as is described in more detail below.

[0031] Referring now to FIG. 3, there is shown a system 50 according to an alternative embodiment of the invention. In place of spectral analyzer 28, system 50 includes a tunable filter 52 that is interposed between lens 24 and a single detector 54, for example, a PMT. In one embodiment, tunable filter comprises a liquid crystal tunable filter (LCTF) that utilizes liquid crystals to continuously vary the retardance of individual filter stages, resulting in a narrow band filter that is electrically tunable over a wide spectral range. Alternatively, the tunable filter 52 may comprise an acousto-optical tunable filter. In any event, tunable filter is controlled by a suitable control unit 56 to vary the bandpass of the filter through the spectral range. At each bandpass, detector 54 receives fluorescence and generates a corresponding electrical output signal, which is converted to digital format by an analog-to-digital converter 58 and then introduced to processor 46 for processing.

[0032] Referring now to FIG. 4, there is shown a system 60 according to still another embodiment of the invention. System 60 includes a long pass dichroic mirror 62 placed in the light stream between the scanning optics 20 and the microscope lens 22. The dichroic mirror 62 is selected such that wavelengths corresponding to the fluorescence radiated by the specimen are reflected by the mirror 62, while the laser light from laser 14 passes through without being reflected. The reflected fluorescence is directed to a focusing lens 64, and then introduced to light guide 26 which delivers the light

to spectral analyzer 28. As described above, spectral analyzer disperses the light and passes the light on to ADC 44, which converts the respective bands into digital signals and introduces the digital signals to processor 46.

**[0033]** System 60 is therefore suitable for use in connection with a non-descanned two-photon microscope. By diverting the radiated fluorescence before it passes through the scanning optics 20, a signal of increased intensity is received by spectral analyzer 28, as compared with a signal that passes through scanning optics 20 and dichroic mirror 18 before being received by a spectral analyzer or detector. Thus, the dwell time at each pixel can be reduced as a result.

**[0034]** Referring now to FIG. 5, a system 70 is shown according to another embodiment of the invention. System 70 includes a light collector 72 that substantially surrounds specimen 12 and includes a reflective inner surface. Thus, light emitted by fluorescent dyes within specimen 12 are collected by the collector, regardless of the direction in which the light radiates. In one embodiment, collector 72 comprises an integrating sphere. Alternatively, collector 72 may be in the shape of an ellipsoid or other structure that substantially encompasses specimen 12 to collect a substantial amount of the light radiating from specimen 12, for example, an elliptical mirror. Collector 72 connects to light guide 26 to deliver the collected light to spectral analyzer 28.

**[0035]** Thus, in use of the various systems described above, laser light is directed by dichroic mirror 18, scanning optics 20, and focusing lens 22 to a region of specimen 12. The photons (either from a single-photon laser or from a multi-photon laser) excite the fluorescent dyes in the region, causing them to fluoresce. The entire emitted spectrum is received and processed simultaneously in certain of the illustrative embodiments to speed up the collection process. The spectral information is then processed to determine the amounts of each dye contributing to the emitted spectrum.

**[0036]** Referring now to FIG. 6, operation of processor 46 is described in greater detail. In one embodiment, processor 46 is programmed to execute a linear unmixing operation upon the incoming spectral data to approximate the quantities of each fluorescent dye that contributed to the emitted spectrum. As shown in FIG. 6, operation begins at step 100 by determining spectral characteristics for the respective individual fluorescent dyes. As is well known in the art, each of the fluorescent dyes emits a particular spectrum over a certain wavelength band and at certain varying intensities within that band (see FIGS. 7a-c which illustrate examples of emissions spectra for three different fluorescent dyes). At step 102, data relating to the probe spectra is recorded in processor memory for subsequent retrieval.

**[0037]** At step 104, processor 46 receives the measured imaging spectrum data from ADC 44 (see FIG. 7d), and retrieves the characteristic spectra for the various fluorescent dyes. At step 106, the measured spectrum is decomposed into the various component dye spectra. This can be accomplished in many different ways. In one embodiment, processor 46 generates a model spectrum from the individual templates, and compares the model spectrum with the actual recorded spectrum. The respective weights of each of the individual templates are then varied to arrive at a close approximation of the actual spectrum. Then, at step 108, processor 46 determines the weights of each dye to quantitate the respective dye intensities.

**[0038]** In another embodiment, processor 46 is programmed to carry out principal component analysis (PCA) on the incoming data. As is well known in the art, PCA is a linear model which transforms the original variables of an emission spectrum into a set of linear combinations of the original

variables called principal components, that account for the variance in the original data set. Suitable forms of PCA algorithms are disclosed in U.S. Pat. Nos. 5,991,653 to Richards-Kortum et al., and 5,887,074 to Lai et al., the disclosures of which are hereby expressly incorporated by reference.

**[0039]** From the foregoing, it will be apparent to those skilled in the art that the present invention provides an efficient and reliable system for receiving and processing emissions spectra in connection with fluorescence microscopy. The system processes the emissions spectra to determine concentrations of plural fluorescent dyes in a particular spectrum, even where the wavelength bands of the dyes overlap.

**[0040]** While the above description contains many specific features of the invention, these should not be construed as limitations on the scope of the invention, but rather as one exemplary embodiment thereof. Many other variations are possible. Accordingly, the scope of the invention should be determined not by the embodiments illustrated, but by the appended claims and their legal equivalents.

What is claimed is:

1. A system, comprising:

- a single photon laser configured to emit radiation capable of exciting a plurality of different excitable markers in a region of a cellular specimen to cause the plurality of different excitable markers to radiate fluorescence;
- a focusing lens configured to focus radiation emitted by the single photon laser on the region of the cellular specimen;
- a dichroic mirror configured to reflect the fluorescence;
- a grating configured to separate the reflected fluorescence into wavelength bands of fluorescence;
- a linear array of high gain photomultiplier tubes configured so that each of the wavelength bands of fluorescence is incident upon a corresponding one of the high gain photomultiplier tubes and so that each of the high gain photomultiplier tubes generates a corresponding analog signal;
- a plurality of digital to analog converters, each digital to analog converter being configured to convert one of the analog signals from the linear array of high gain photomultiplier tubes to a digital signal; and
- a processor configured to linearly unmix the digital signals.

2. The system of claim 1, wherein the dichroic mirror is configured so that radiation from the single photon laser that is reflected from the specimen passes through the dichroic mirror.

3. The system of claim 1, wherein the processor is configured to identify the contribution to the fluorescence from each of the plurality of excitable markers.

4. A system, comprising:

- a single photon laser microscope operative to cause a plurality of different excitable markers in a region of a cellular specimen to radiate fluorescence;
- photomultiplier tubes, each of the plurality of photomultiplier tubes being configured to receive a corresponding wavelength band of the fluorescence so that each of the photomultiplier tubes generates a corresponding analog signal;
- a plurality of digital to analog converters, each digital to analog converter being configured to convert one of the analog signals from the linear array of high gain photomultiplier tubes to a digital signal; and
- a processor configured to unmix the digital signals.

5. The system of claim 4, wherein the single photon laser microscope comprises a single photon laser configured to emit the radiation.

6. The system of claim 5, further comprising a focusing lens configured to focus the radiation to the region of the cellular specimen.

7. The system of claim 4, further comprising a dichroic mirror configured to reflect the fluorescence.

8. The system of claim 7, wherein the dichroic mirror is configured so that radiation from the single photon laser that is reflected from the specimen passes through the dichroic mirror.

9. The system of claim 4, further comprising a grating configured to separate the fluorescence into wavelength bands of fluorescence.

10. The system of claim 4, wherein the photomultiplier tubes form a linear array.

11. The system of claim 10, wherein the photomultiplier tubes are high gain photomultiplier tubes.

12. The system of claim 4, wherein the photomultiplier tubes are high gain photomultiplier tubes.

13. The system of claim 4, wherein the processor is configured to linearly unmix the digital signals.

14. The system of claim 4, wherein the processor is configured to identify the contribution to the fluorescence from each of the plurality of excitable markers.

15. A method, comprising:

using the system of claim 1 to monitor cellular activity in a cellular specimen.

16. A method, comprising:

using the system of claim 3 to monitor cellular activity in a cellular specimen.

17. A method, comprising:

applying a plurality of different excitable markers to a cellular specimen;

applying light to the cellular specimen from a single-photon laser microscope to cause fluorescence to be radiated from the region by markers in that region of the cellular specimen;

using a grating to separate the fluorescence into wavelength bands of fluorescence; and

using a linear array of photomultiplier tubes to detect the fluorescence, each photomultiplier tube receiving one of the wavelength bands of fluorescence and generating a corresponding analog signal;

converting the analog signals to digital signals; and linearly unmixing the digital signals.

18. The method of claim 17, further comprising identifying the contribution to the fluorescence from each of the plurality of excitable markers.

19. A method, comprising:

applying light from a single-photon laser to a region of a cellular specimen having a plurality of different excitable markers, thereby causing fluorescence to be radiated from the region of the cellular specimen;

separating the fluorescence into wavelength bands of fluorescence using a grating; and

detecting the fluorescence via photomultiplier tubes, each photomultiplier tube receiving one of the wavelength bands of fluorescence and generating a corresponding analog signal;

converting the analog signals to digital signals; and linearly unmixing the digital signals.

20. The method of claim 19, further comprising applying the plurality of different excitable markers to the cellular specimen.

21. The method of claim 19, wherein the single photon laser is part of a single photon laser microscope.

22. The method of claim 19, wherein the photomultiplier tubes form a linear array.

23. The method of claim 22, wherein the photomultiplier tubes are high gain photomultiplier tubes.

24. The method of claim 19, wherein the photomultiplier tubes are high gain photomultiplier tubes.

25. The method of claim 19, further comprising identifying the contribution to the fluorescence from each of the plurality of excitable markers.

26. A system, comprising:

a single photon laser configured to emit radiation capable of exciting a plurality of different excitable markers in a region of a cellular specimen to cause the plurality of different excitable markers to radiate fluorescence;

a focusing lens configured to focus radiation emitted by the single photon laser on the region of the cellular specimen;

a dichroic mirror configured to reflect the fluorescence;

a grating configured to separate the reflected fluorescence into wavelength bands of fluorescence;

a linear array of high gain photomultiplier tubes configured so that each of the wavelength bands of fluorescence is incident upon a corresponding one of the high gain photomultiplier tubes and so that each of the high gain photomultiplier tubes generates a corresponding analog signal;

a plurality of digital to analog converters, each digital to analog converter being configured to convert one of the analog signals from the linear array of high gain photomultiplier tubes to a digital signal; and

a processor configured to identify the contribution to the fluorescence from each of the plurality of excitable markers.

27. A system, comprising:

a single photon laser microscope operative to cause a plurality of different excitable markers in a region of a cellular specimen to radiate fluorescence;

photomultiplier tubes, each of the plurality of photomultiplier tubes being configured to receive a corresponding wavelength band of the fluorescence so that each of the photomultiplier tubes generates a corresponding analog signal;

a plurality of digital to analog converters, each digital to analog converter being configured to convert one of the analog signals from the linear array of high gain photomultiplier tubes to a digital signal; and

a processor configured to identify the contribution to the fluorescence from each of the plurality of excitable markers.

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