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(54) **COPOLYMERES d' $\epsilon$ -CAPROLACTONE, DE GLYCOLIDE ET  
D'ACIDE GLYCOLIQUE POUR LE REVETEMENT DE  
SUTURES**

(54) **COPOLYMERS OF  $\epsilon$ -CAPROLACTONE, GLYCOLIDE AND  
GLYCOLIC ACID FOR SUTURE COATING**

(57) Copolymer of a predominant amount: of  $\epsilon$ -caprolactone, the balance being glycolide and glycolic acid. Coating for an absorbable, multifilament surgical suture prepared by dissolving the copolymer in an organic solvent.

ABSTRACT

Copolymer of a predominant amount of  $\epsilon$ -caprolactone,  
the balance being glycolide and glycolic acid. Coating for  
5 an absorbable, multifilament surgical suture prepared by  
dissolving the copolymer in an organic solvent.

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TITLE OF INVENTION

COPOLYMERS OF  $\epsilon$ -CAPROLACTONE, GLYCOLIDE AND GLYCOLIC ACID  
FOR SUTURE COATING

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BACKGROUND OF THE INVENTION

This invention relates to copolymers of  
 $\epsilon$ -caprolactone and glycolide, and more specifically, to  
10 such copolymers with improved properties especially  
adapted for use as coatings for absorbable multifilament  
surgical sutures.

Multifilament surgical sutures such as Vicryl®  
15 poly(lactide-co-glycolide) multifilament suture typically  
require a surface coating to improve the pliability and  
knotting characteristics of the suture. A polymer coating  
which has recently been developed and shows significant  
promise as a suture coating is derived from a polymer  
20 solution of  $\epsilon$ -caprolactone in an appropriate organic  
solvent. The coating solution is typically applied to the  
surface of the suture using conventional techniques, and  
then the solvent is removed. Polycaprolactone is a  
biocompatible polymer with a relatively low melting point,  
25 a property which is essential for good coating  
characteristics. Additionally, sutures coated with  
polycaprolactone exhibit enhanced pliability and handling  
characteristics. Unfortunately, polycaprolactone  
homopolymer is essentially nonabsorbable because it  
30 retains some of its mass and mechanical integrity in vivo  
for periods up to one year, which is too long for numerous  
surgical applications.

In an effort to improve the bioabsorbability and other  
35 properties of a polycaprolactone coating polymer, the

polymer composition has been modified by incorporating copolymerizable monomers or lubricating agents therein. For example, U.S. Patent 4,624,256 discloses a suture coating copolymer of at least 90 percent  $\epsilon$ -caprolactone and a biodegradable monomer, and optionally a lubricating agent. Examples of monomers for biodegradable polymers disclosed include glycolic acid and glycolide, as well as other well known monomers typically used to prepare polymer fibers or coatings for multifilament sutures. U.S. Patent 4,791,929 discloses a bioabsorbable coating of a copolymer of at least 50 percent  $\epsilon$ -caprolactone and glycolide. Sutures coated with such copolymers are reported to be less stiff than sutures coated with other materials, and the physical properties of the coated suture are also reported to be acceptable.

Unfortunately, the problem of adequate bioabsorbability of homopolymers and copolymers of  $\epsilon$ -caprolactone for suture coating applications still remains. One of the difficulties a skilled polymer chemist has faced in solving this problem is in developing a faster absorbing polymer of  $\epsilon$ -caprolactone without sacrificing the physical properties of multifilament sutures coated with such a polymer. In view of the deficiencies with the known art polycaprolactone coatings, it would be most desirable to accomplish this goal.

#### SUMMARY OF THE INVENTION

In one aspect, the invention is a copolymer of a predominant amount of  $\epsilon$ -caprolactone, and the balance glycolide and glycolic acid. The copolymer is characterized by a concentration of glycolic acid such that the intrinsic viscosity of the copolymer in

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hexafluoroisopropyl alcohol (HFIP) is between about 0.15 to about 0.60 deciliters per gram (dl/g).

5 In another aspect, the invention is a coating for a surgical suture. This coating comprises a solution of the copolymer described above in an organic solvent.

10 Surprisingly, the use of glycolic acid as a comonomer into the copolymers of this invention increases the rate of absorption of the copolymers relative to the absorption rate of prior art copolymers of  $\epsilon$ -caprolactone and glycolide. This increase in the rate of absorption is achieved while maintaining the physical properties of sutures coated with such copolymers, for example, tissue  
15 drag, which measures the degree of trauma associated with passing the coated suture through tissue, knot tiedown characteristics and tensile properties.

20 The copolymers of this invention and the coatings derived therefrom can be used for coating bioabsorbable, multifilament surgical sutures.

#### DETAILED DESCRIPTION OF THE INVENTION

25 A predominant amount of  $\epsilon$ -caprolactone generally refers to an amount of  $\epsilon$ -caprolactone greater than 50 mole percent of the comonomer composition from which the copolymer of this invention is derived.  $\epsilon$ -Caprolactone is the predominant component of the copolymer because of its  
30 low melting temperature and its ability to enhance the physical properties of coated multifilament sutures. Preferably, the amount of  $\epsilon$ -caprolactone used ranges from about 80 to about 95, more preferably from about 90 to about 95 mole percent.

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The remaining comonomers of the copolymer of this invention are glycolide and glycolic acid. The amount of glycolic acid in the comonomer composition from which the copolymer is derived is an amount such that the intrinsic viscosity of the copolymer in a 0.1 g/dl solution of HFIP at 25°C is between about 0.15 to about 0.60 dl/g. Preferably, the intrinsic viscosity of the copolymer is between about 0.20 to about 0.50 dl/g. The glycolic acid can be used in part to control the molecular weight of the copolymer, and therefore its intrinsic viscosity, and, in combination with the glycolide comonomer, can be used to lower the melting temperature of the copolymer relative to that of a polycaprolactone homopolymer. Advantageously, the crystalline melting temperature of the copolymer is between about 30 to about 60°C, preferably between about 35 to about 50°C. The frequency of the hydrolytically labile linkages associated with the use of glycolic acid along the chains of the copolymer is also responsible for enhancing the absorption profile of the coating.

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The adjustment of the intrinsic viscosity of the copolymer by varying the concentration of glycolic acid is important to achieve a copolymer coating that will not only form a film on the outer surface of the suture but also penetrate and distribute evenly into the interstices of the multifilament fibers. This penetration and the subsequent adsorption of the coating polymer onto individual fibers of the multifilament increases the pliability of the suture and enhances its knotting characteristics, specifically the ease with which a knot can slide down the length of the suture during an operative procedure. Likewise, the control of the crystalline melting temperature, which to a significant degree is controlled by the intrinsic viscosity, by varying the relative proportions of glycolide and glycolic

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acid is important to achieve similar improvements in the properties of coated sutures.

Advantageously, the amount of glycolic acid in the comonomer composition from which the copolymer is derived to achieve an acceptable intrinsic viscosity and to increase the rate of absorption relative to the prior art copolymers of  $\epsilon$ -caprolactone and glycolide ranges from about 1 to about 15, preferably from about 2 to about 10 mole percent. The glycolide comonomer not only lowers the melting temperature of the copolymer, but also, to a lesser extent relative to glycolic acid, increases the rate of absorption and is preferably present in the comonomer composition at a concentration ranging from about 5 to about 20, more preferably from about 5 to about 10 mole percent. The mole ratio of glycolide to glycolic acid to achieve desired coating properties advantageously ranges from about 20:80 to about 95:5, preferably from about 70:30 to about 90:10.

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The copolymers of this invention can be prepared by polymerizing in the presence of an organometallic catalyst the desired amounts of  $\epsilon$ -caprolactone, glycolide and glycolic acid at an elevated temperature, e.g. 160 to 190°C, for a time sufficient to achieve the desired intrinsic viscosity. The organometallic catalyst is preferably a tin-based catalyst, preferably stannous octoate, and is present in the reaction mixture at a mole ratio of monomer to catalyst between 10,000 to 90,000 to 1, preferably 15,000 to 30,000 to 1.

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The organic solvent for the polymer coating of this invention is advantageously a solvent which has a normal boiling point no greater than 120°C. Examples of suitable organic solvents include but are not limited to

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chlorinated aliphatic solvents such as 1,1,2-trichloroethane, aromatic solvents such as toluene, and aliphatic ketones such as acetone.

5           The coating can easily be prepared by simply  
dissolving the copolymer of this invention into the  
appropriate organic solvent. The concentration of the  
copolymer in solution desirably ranges from about 1 to  
about 20, preferably from about 10 to about 15 weight  
10 percent. Generally, concentrations greater than 20 weight  
percent polymer provide coating solutions which are too  
viscous to achieve adequate penetration of the coating  
solution into the interstices of the fibers, and  
concentrations below 1 weight percent are inadequate to  
15 properly coat a sufficient amount of copolymer onto the  
suture, although it may be possible but inconvenient to  
employ two or more coating steps to achieve a sufficient  
coating concentration on the copolymer. Once a solution  
of the copolymer is prepared, a suture can be coated using  
20 conventional coating techniques, e.g. dipping, spraying,  
etc. After the coating is applied, the solvent can be  
removed by drying in air, or by other techniques well  
known in the art, for example, removing the solvent at an  
elevated temperature under vacuum.

25           The suture to be coated can be a monofilament or  
multifilament suture. Preferably, a multifilament suture  
in a braided, twisted, crocheted, knitted or covered form  
is used. Preferably, the suture is an absorbable,  
30 multifilament braided suture. The preferred absorbable  
sutures are those prepared from a polymer of a lactone or  
a polymer of one or more lactones. Examples of the most  
widely used lactones for suture preparation are lactide,  
glycolide and  $\epsilon$ -caprolactone. The most preferred suture  
35 is Vicryl® poly(lactide-co-glycolide) multifilament

braided suture. For numerous surgical applications, the suture is attached to one or more needles.

The following examples illustrate the claimed invention and are in no way intended to limit its scope.

EXAMPLE 1

COPLOYMER OF  $\epsilon$ -CAPROLACTONE/GLYCOLIDE/GLYCOLIC ACID  
AT 0.90/0.05/0.10 MOLE RATIO

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A flame dried, 250 ml, round bottom single neck flask is charged with 102.73g (0.9 mole) of  $\epsilon$ -caprolactone, 5.80g (0.05 mole) of glycolide, 7.61g (0.10 mole) of glycolic acid, and 0.121 milliliters of stannous octoate (0.33 molar in toluene). The flask is fitted with a flame dried mechanical stirrer. The reactor is purged with nitrogen three times before venting with nitrogen. The reaction mixture is heated to 160°C and maintained at this temperature for 24 hours. The copolymer is isolated, characterized, and tested for absorption. The results are reported in Table 1.

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EXAMPLE 2

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COPOLYMER OF  $\epsilon$ -CAPROLACTONE/GLYCOLIDE/GLYCOLIC ACID  
AT 0.90/0.08/0.04 BY MOLE

The procedure of Example 1 is repeated, except that the reaction flask is charged with 9.29g (0.08 mole) of glycolide and 3.04g (0.04 mole) of glycolic acid.

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COMPARATIVE EXAMPLE 1COPOLYMER OF  $\epsilon$ -CAPROLACTONE/GLYCOLIDE AT 90/10 BY WT.  
(90/10 BY MOLE)

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A flame dried, 250 ml, round bottom, single neck flask is charged with 90g (0.789 mole) of  $\epsilon$ -caprolactone, 10g (0.0862 mole) of glycolide, 7.96 ml (40 millimole/mole of total monomer) of distilled 1-dodecanol, and 0.121 ml of stannous octoate (0.33 molar solution in toluene). The reaction flask is purged with nitrogen three times before venting with nitrogen. The reaction mixture is heated to 180°C and maintained there for 4.5 hours. The copolymer is isolated, characterized, and tested for absorption. The results are reported in Table 1.

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TABLE 1

CHARACTERIZATION AND ABSORPTION OF COATING COPOLYMERS

<u>Example No.</u>	<u>1</u>	<u>2</u>	<u>Comparative Example 1</u>
<u>Characterization</u>			
Copolymer comp. caprolactone/glycolide/GA <sup>1</sup>	90/5/10 by mole	90/8/4 by mole	90/10/0 by wt. (90/10/0 by mole)
Intrinsic Viscosity of copolymer in HFIP, dl/g	0.19	0.31	0.28
Melting Point <sup>2</sup>	41-44°C	42-40°C	35-45°C
<u>Absorption</u>			
In Vitro hydrolysis at 100°C (sterile water)			
Percent nonhydrolyzed copolymer <sup>3</sup> at			
2 days	19.79	25.76	77.23
2 days (repeat)	15.82	35.23	81.80

- <sup>1</sup> Glycolic acid
- <sup>2</sup> Determined by hot stage microscopy
- <sup>3</sup> Determined by measuring weight loss of copolymer after the indicated number of days

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The data from Table 1 shows a significant increase in the rate of hydrolysis for the copolymers of this invention compared to prior art copolymers of  $\epsilon$ -caprolactone and glycolide. The rate of hydrolysis is a measure of the rate of absorption since synthetic copolymers degrade via hydrolysis.

A 10 and 15 percent coating solution of each of the copolymers of Examples 1 and 2, and Comparative Example 1, in toluene is prepared. A size 2/0 (USP standard) Vicryl® poly(lactide-co-glycolide) braided multifilament suture is coated with each coating solution using conventional laboratory coating equipment. The physical properties of the coated sutures are evaluated and the results are reported in Table 2 as Examples 3, 4, and Comparative Example 2, which correspond to Examples 1, 2, and Comparative Example 1, respectively.

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TABLE 2

PHYSICAL PROPERTIES OF SUTURES COATED WITH COPOLYMERS

Example No.	3	4	Comparative Example 2
	10% Sol. caprolactone/ glycolide/GA <sup>1</sup> Copolymer	15% Sol. caprolactone/ glycolide/GA <sup>1</sup> copolymer	15% Sol. caprolactone/ glycolide/GA <sup>1</sup> copolymer
	90/5/10 by mole IV = 0.19 dl/g	90/8/4 by mole IV = 0.31 dl/g	90/10/0 by wt. (90/10/0 by mole) IV = 0.28 dl/g
Dia., (mils)	12.6	12.7	12.9
Tissue Drag <sup>2</sup> , gms	18.34	22.13	32.25
Wet Roughness Tiedown <sup>3</sup> , gms	310.32	353.98	149.66
Percent Elong. <sup>4</sup>	17.7	18	17.3
Dry Knot Tensile <sup>4</sup> , psi	73,800	72,600	71,900
Wet Knot Tensile <sup>4</sup> , psi	75,400	71,800	71,900
Dry Str. Tensile <sup>4</sup> , psi	124,300	121,600	112,500

<sup>1</sup> Glycolic acid

<sup>2</sup> Tissue Drag is a measure of the relative smoothness of the suture while passing through tissue, and is determined by using an Instron Tensile Tester and a recording device.

<sup>3</sup> Tiedown measured on a Table-Model Instron Tensile Tester as describe in U.S. Patent No. 3,942,532.

<sup>4</sup> Tensile properties and elongation determined generally according to the procedures outlined in U.S. Patent No. 4,838,267. Wet tensile properties were measured after immersing the coated suture in water at 25°C for 24 hours.

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The data from Table 2 illustrates comparable physical properties achieved for sutures coated with the copolymers of this invention relative to the physical properties of sutures coated with prior art copolymers of  $\epsilon$ -caprolactone and glycolide.

Similar outstanding results can be obtained by varying the mole ratio of each of the comonomer components of the copolymer. A coated suture with tailor-made properties can be prepared by selecting an appropriate multifilament suture with the desired coating copolymer.

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The embodiments of the invention in which an exclusive property or privilege is claimed are defined as follows:

1. A copolymer of a predominant amount of  $\epsilon$ -caprolactone and the balance glycolide and glycolic acid, at a concentration of glycolic acid such that the intrinsic viscosity of the copolymer in HFIP is between about 0.15 to about 0.60 dl/g.
2. The copolymer of claim 1 wherein the amount of  $\epsilon$ -caprolactone is between about 80 to about 95 mole percent.
3. The copolymer of claim 2 wherein the amount of  $\epsilon$ -caprolactone is between about 90 to about 95 mole percent.
4. The copolymer of claim 3 wherein the intrinsic viscosity of the copolymer is between about 0.20 to about 0.50 dl/g.
5. The copolymer of claim 4 wherein the melting temperature of the copolymer is between about 35 to about 50°C.
6. The copolymer of claim 5 wherein the amount of glycolic acid is between about 1 to about 15 mole percent.
7. The copolymer of claim 6 wherein the amount of glycolide is between about 2 to about 10 mole percent.
8. A coating for a surgical suture comprising a solution of the copolymer of claim 1 or 7 in an organic solvent.
9. The coating of claim 8 wherein the amount of copolymer in solution is between about 1 to about 20 weight percent.

10. The coating of claim 9 wherein the suture is an absorbable monofilament or multifilament suture with or without an attached needle.
- 5 11. The coating of claim 10 wherein the suture is an absorbable multifilament suture.
12. The coating of claim 11 wherein the absorbable multifilament suture is in the form of a braid.
- 10 13. The coating of claim 12 wherein the suture is prepared from a polymer of a lactone or one or more lactones.
- 15 14. The coating of claim 13 wherein the multifilament suture is a poly(lactide-co-glycolide) braided multifilament suture.
- 20 15. An absorbable multifilament suture coated with the copolymer of claim 1.
16. An absorbable multifilament suture coated with the copolymer of claim 7.

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