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(71) Applicant(s):  
**Lab901 Limited**  
**(Incorporated in the United Kingdom)**  
**Unit 53 Imex Business Centre,**  
**Dryden Road, Bilston Glen, LOANHEAD,**  
**Midlothian, EH20 9LZ, United Kingdom**

(continued on next page)

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**US 20050220675 A1**

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INT CL **B01F, B01L, B81B, F15C, G01N**  
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(54) Abstract Title: **Analysis instrument**

(57) The invention relates to an analysis instrument for processing a microfluidic device 1, comprising sample storage means 26, a microfluidic device holder 21, sample loading means 30 for loading sample into a microfluidic device disposed in the holder, processing means for enabling a reaction in a microfluidic device 22, and detection means for detecting and/or measuring the reaction 41, characterised in that the microfluidic device holder is adapted to hold the microfluidic device comprising or including a tape in position for processing and/or detection.

A second invention disclosed relates to a microfluidic processing device, comprising a reaction chamber, a sample loading chamber into which a sample is injectable, the reaction chamber being operatively connected to the sample loading chamber, a cover that extends across at least part of the sample loading chamber, the cover and the reaction chamber comprising pierceable material and being separated by an overspill cavity configured to accept any overspill of an injected sample.

Finally, the invention concerns a kit comprising an analysis instrument and a microfluidic processing device as described above.

The device holder 21, a electrical probe block assembly 22, pipette tip holder 23 and micro-titer sample storage plate 26 are mounted on a moveable platform 27. Above the moveable platform 27 is a fixed gantry beam 36 which carries a pump 30, to inject a sample into the microfluidic device, and a piercing tool to break the pierceable material of the device. The detection means 41 may comprise a CCD camera assembly and processing can comprise fractionation, isolation, purification, PCR, biomolecular separation, molecular binding and isolation or retrieval of reaction and products.

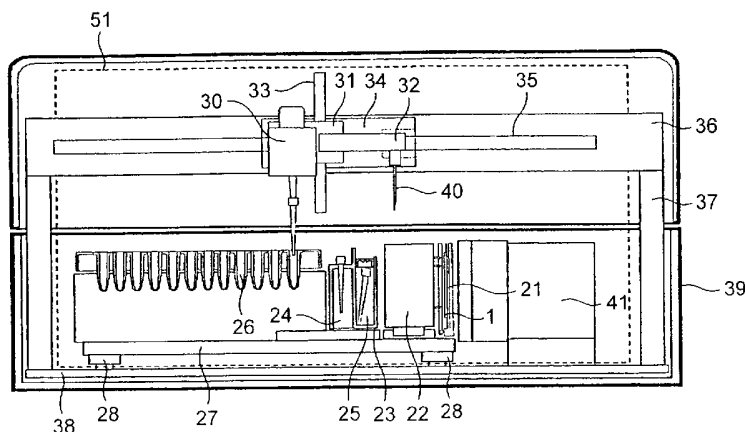


FIG. 3A

**GB 2422796 A continuation**

(72) Inventor(s):

**Stuart Polwart  
Joel Fearnley  
Kenneth G Macnamara  
Urs Lamb**

(74) Agent and/or Address for Service:

**R G C Jenkins & Co  
26 Caxton Street, London, SW1H 0RJ,  
United Kingdom**

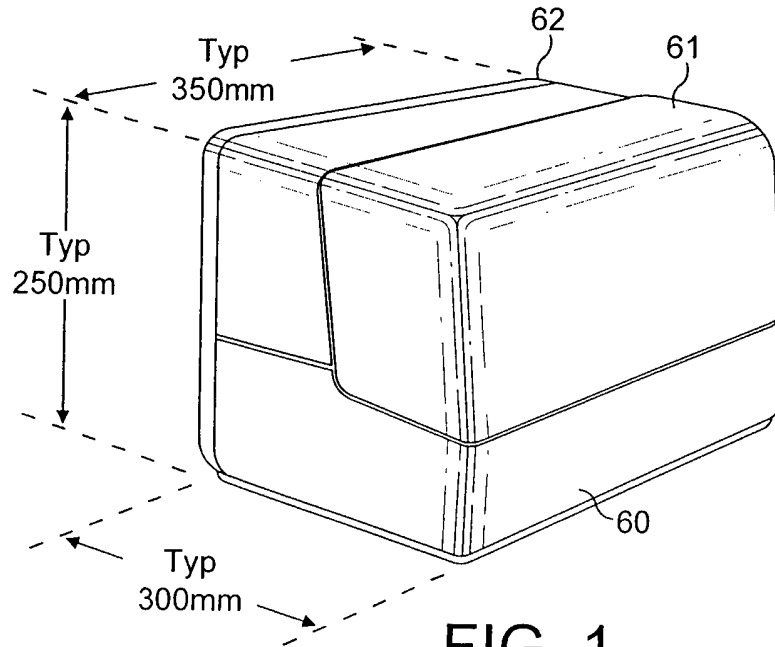


FIG. 1

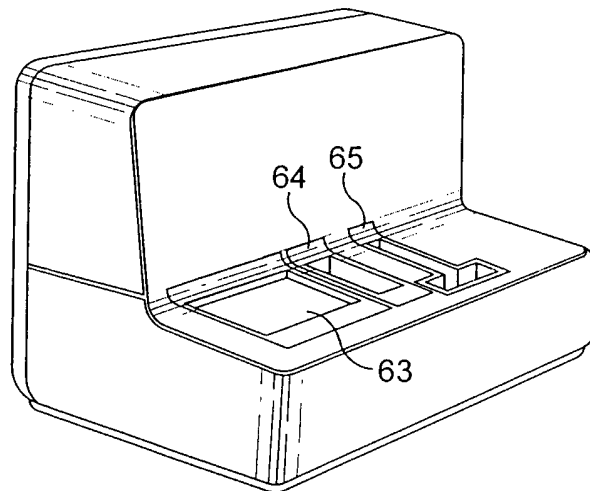


FIG. 2

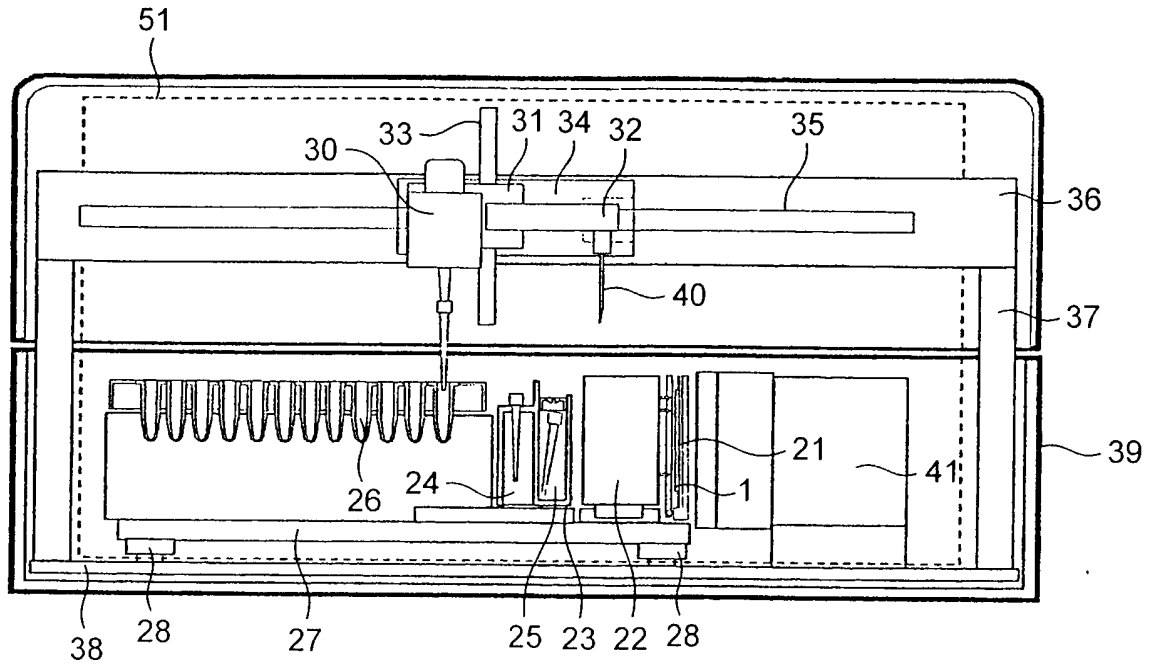


FIG. 3A

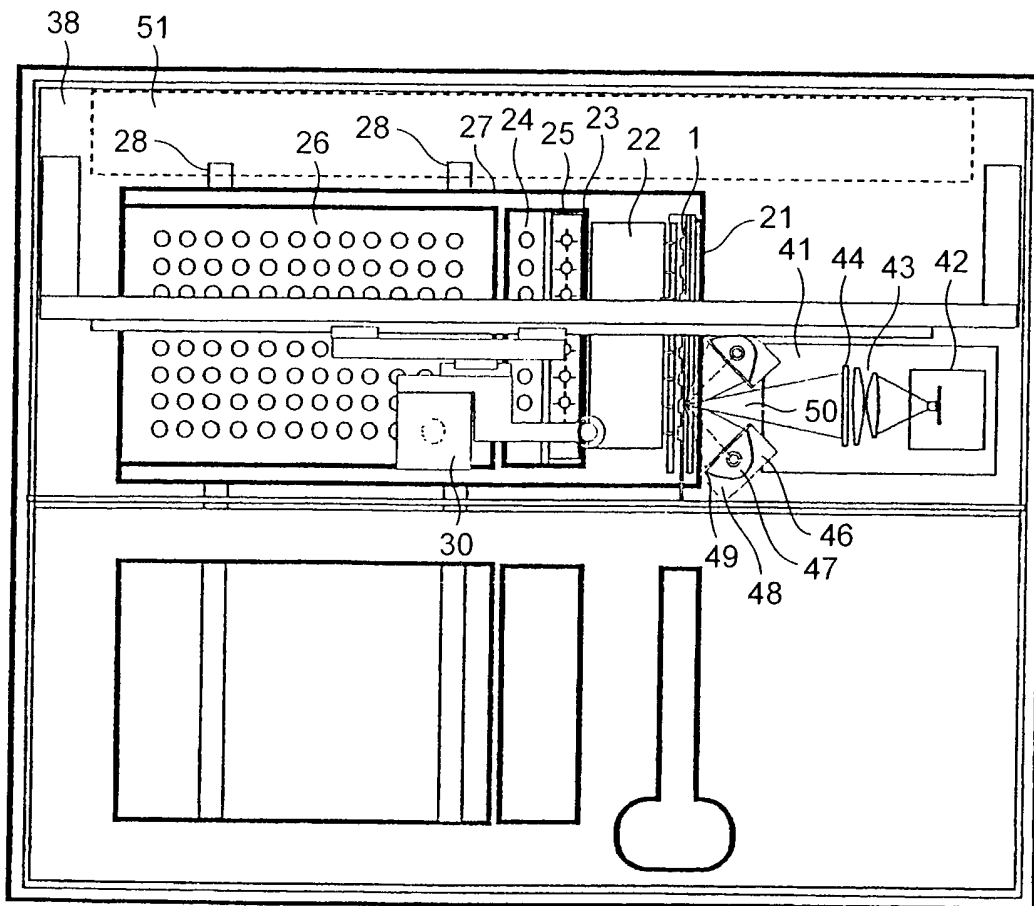


FIG. 3B

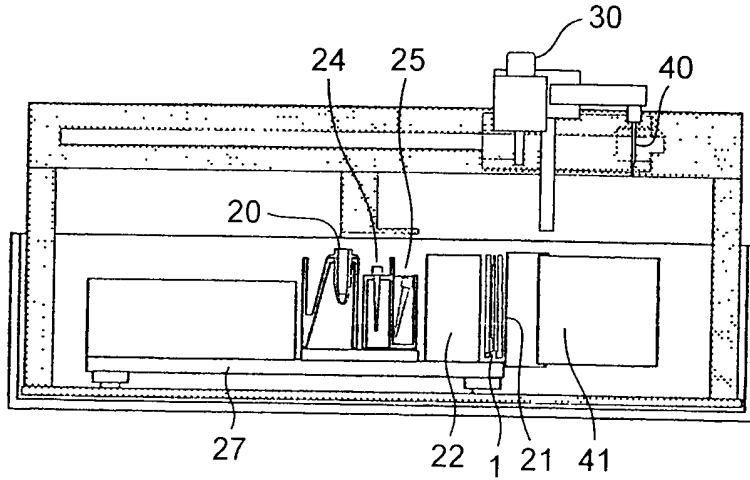


FIG. 4A

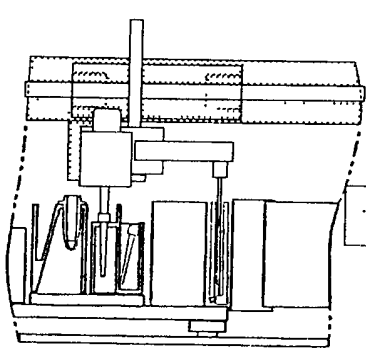


FIG. 4B

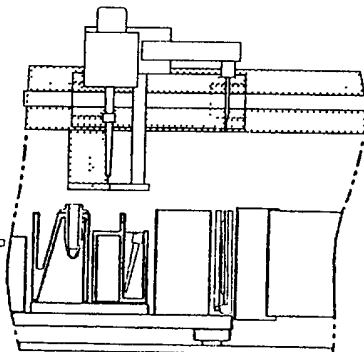


FIG. 4C

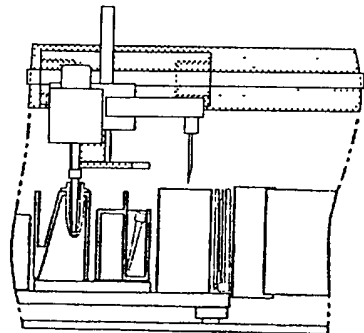


FIG. 4D

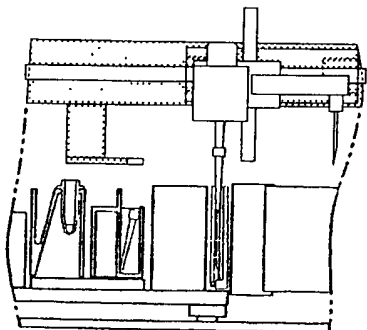


FIG. 4E

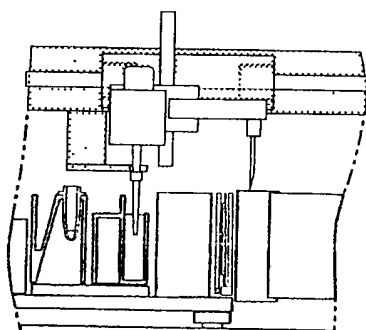


FIG. 4F

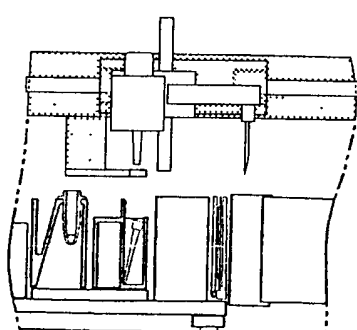


FIG. 4G

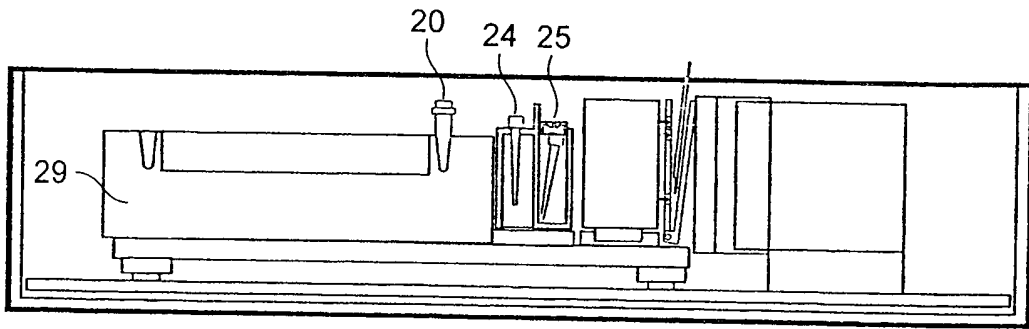


FIG. 5A

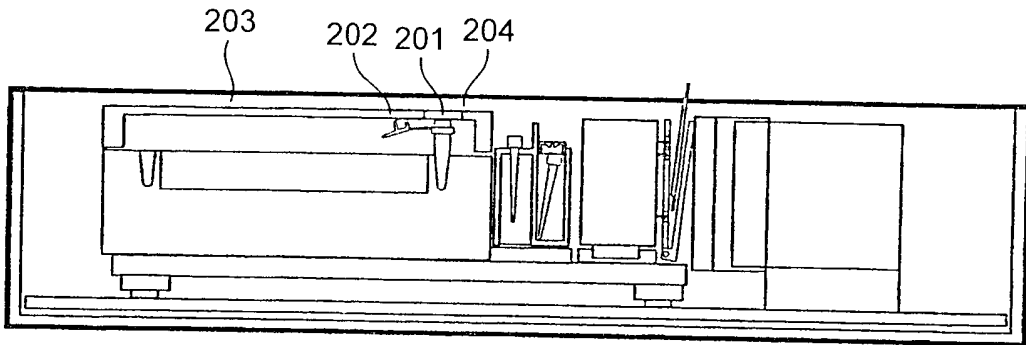


FIG. 5B

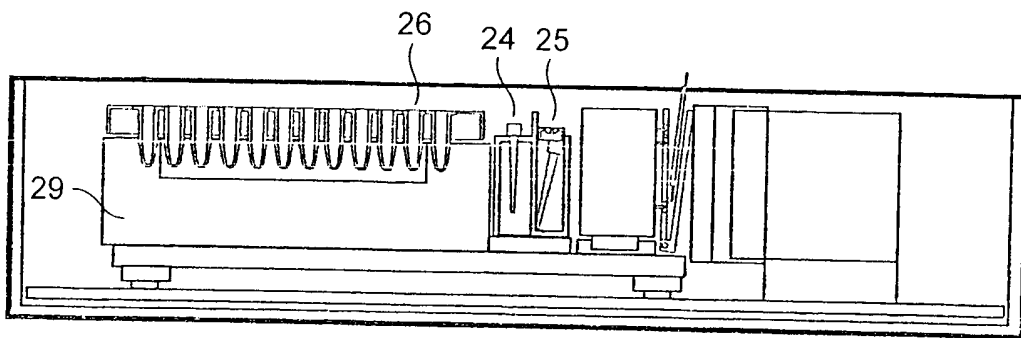


FIG. 5C

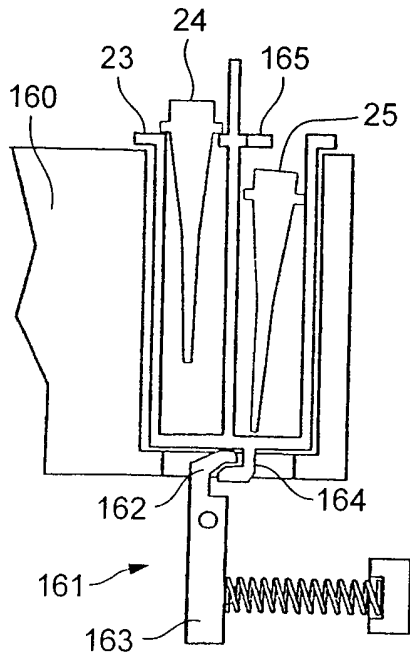


FIG. 6A

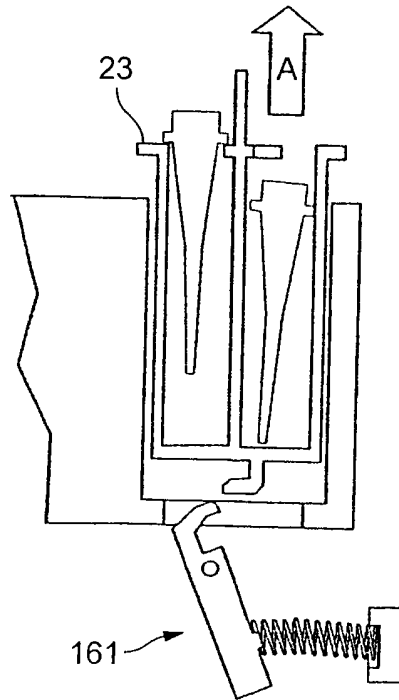


FIG. 6B

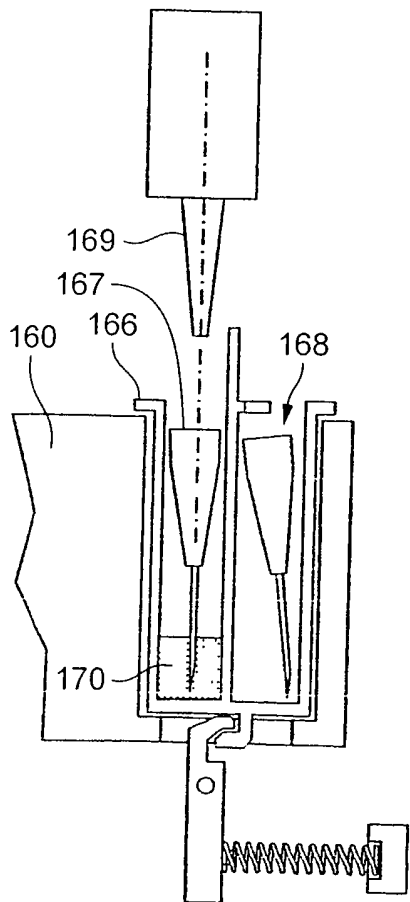


FIG. 6C

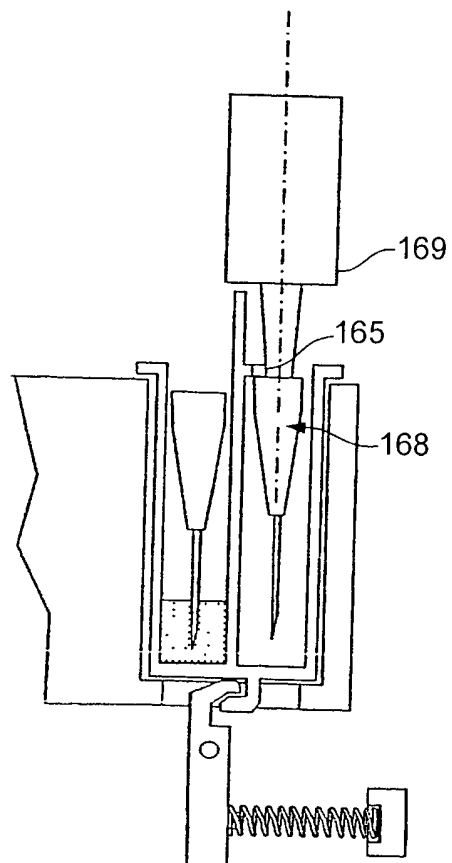


FIG. 6D

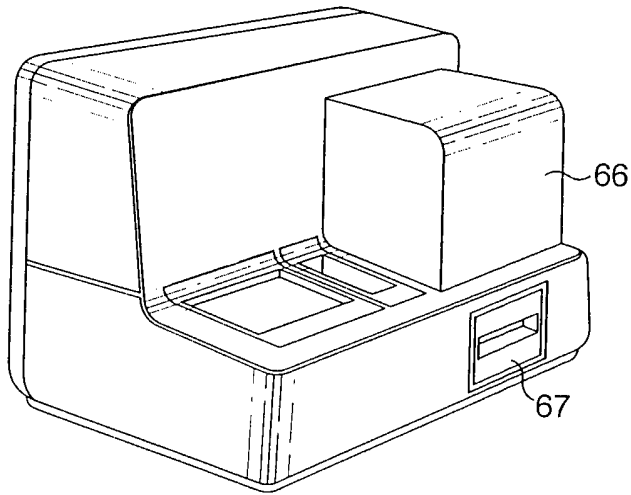


FIG. 7

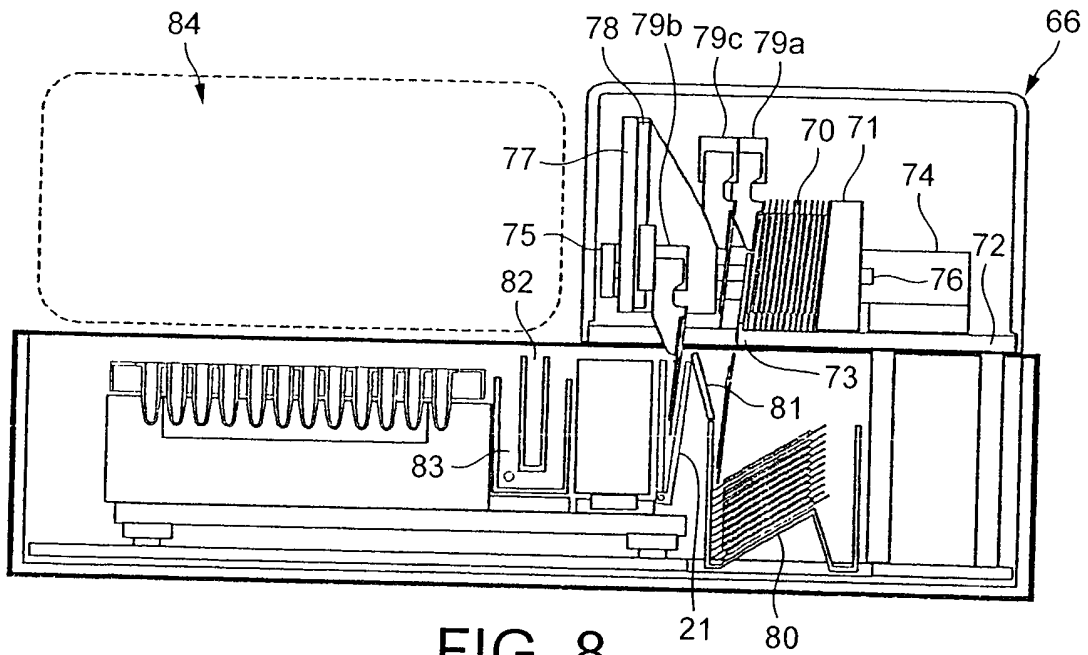


FIG. 8



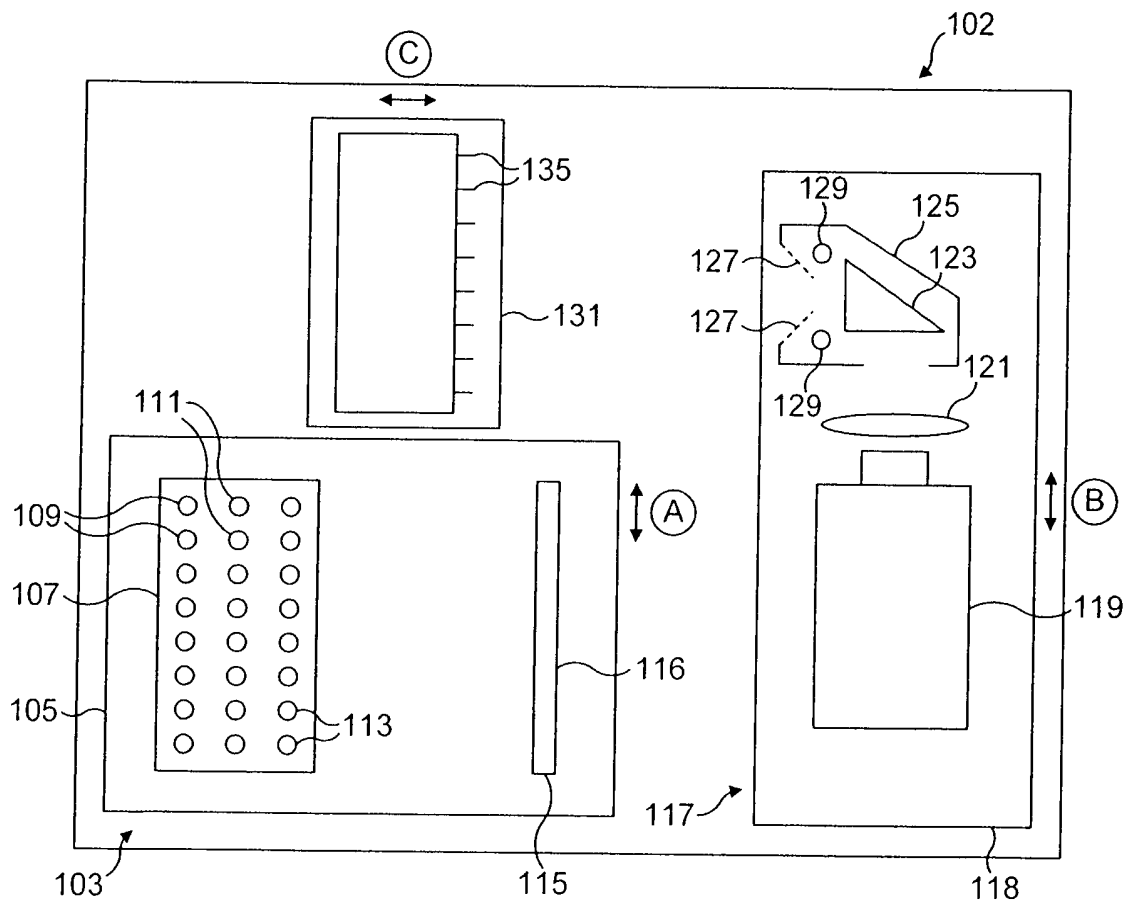


FIG. 9

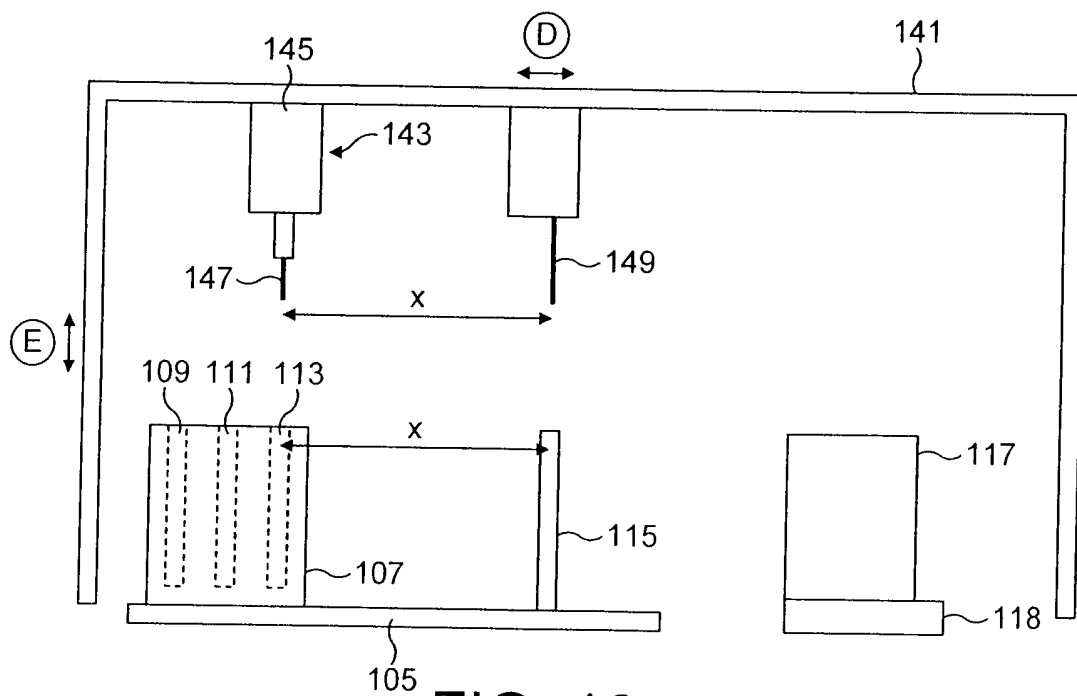


FIG. 10

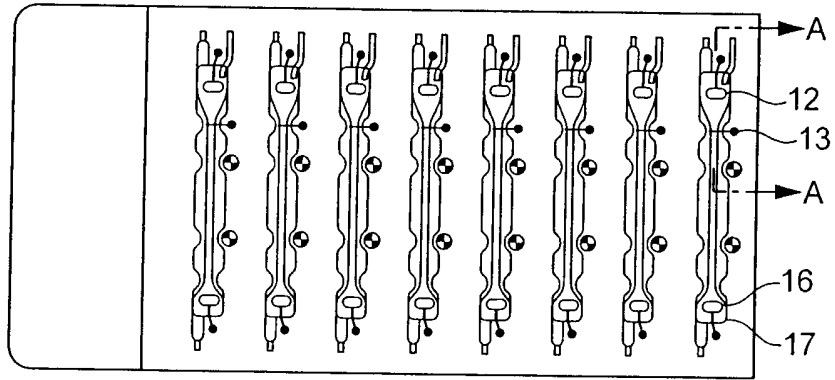


FIG. 11

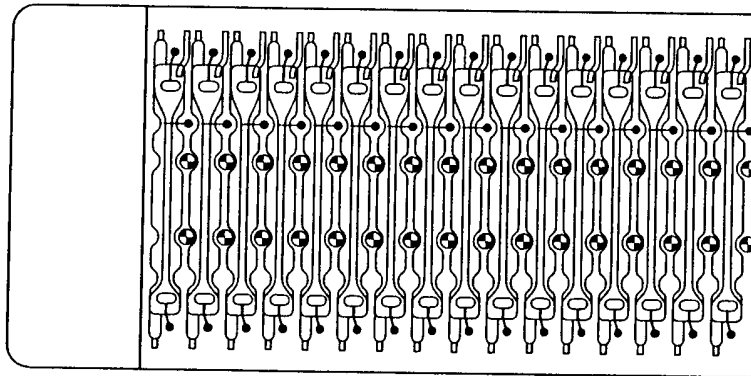


FIG. 12

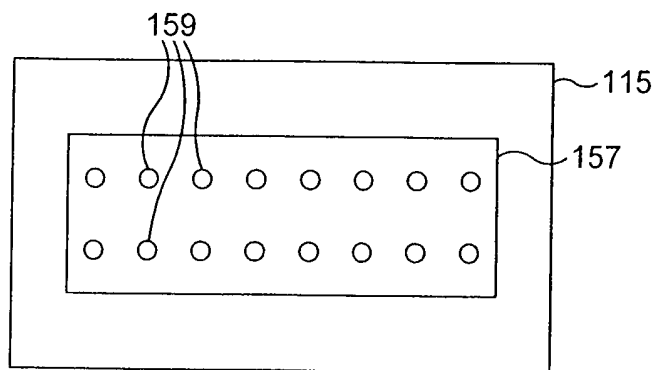


FIG. 13

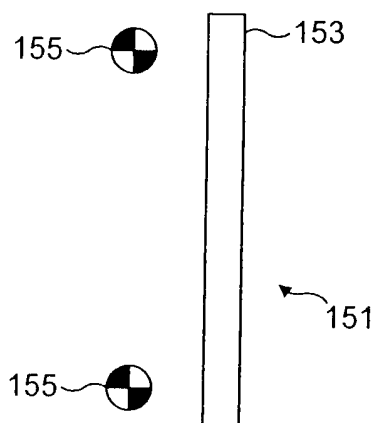


FIG. 14

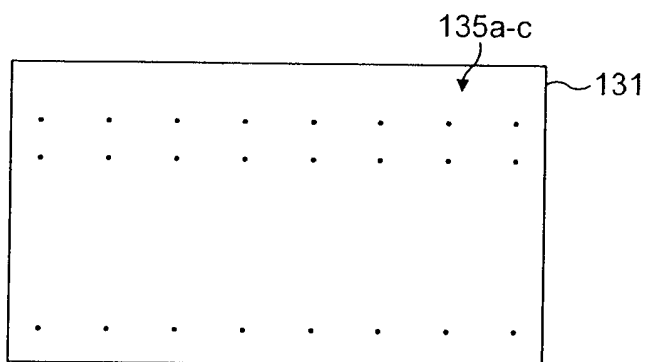
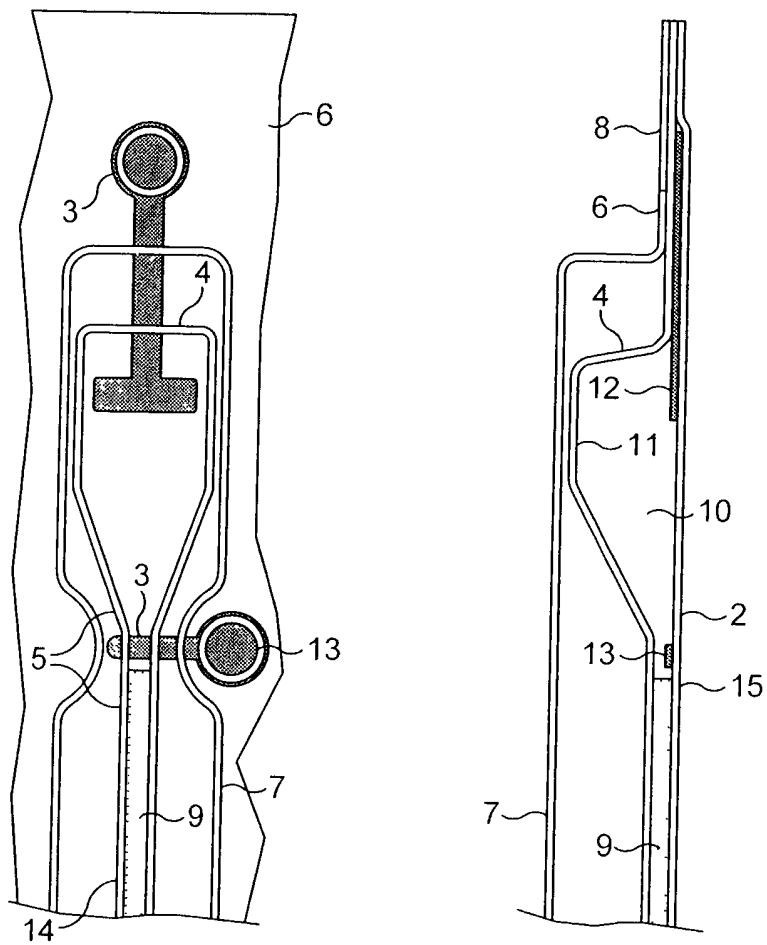


FIG. 15



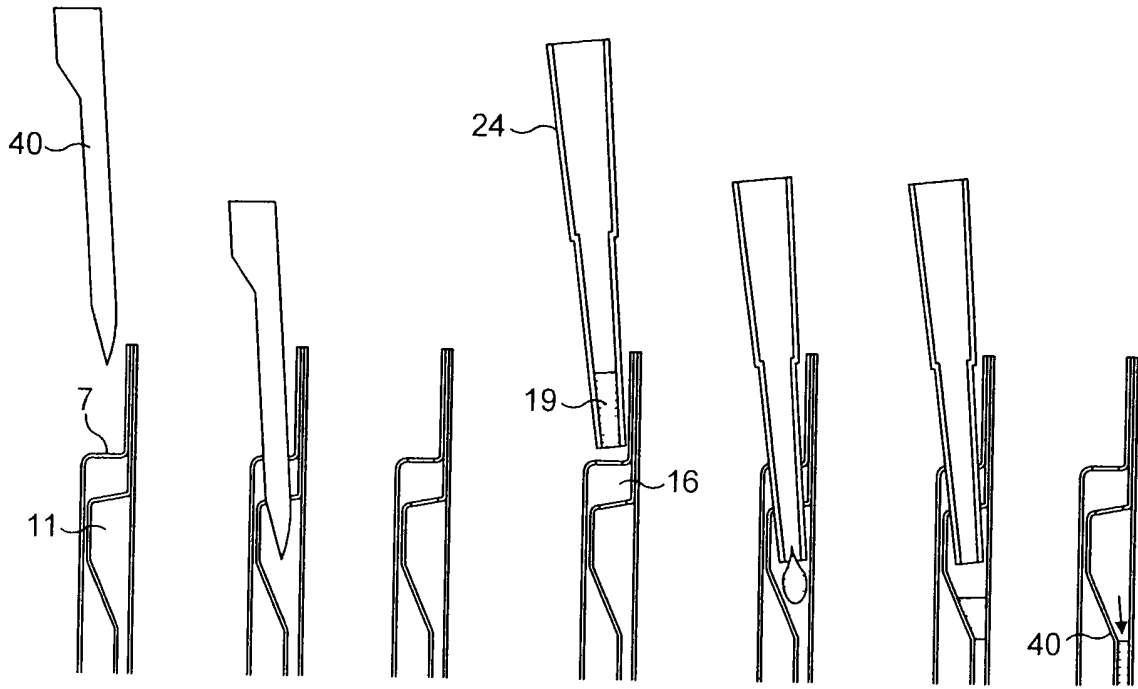


FIG. 17a

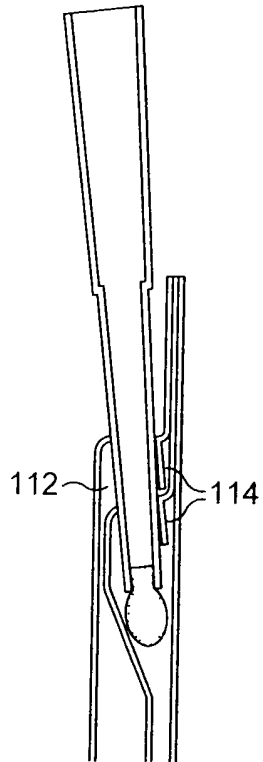


FIG. 17b

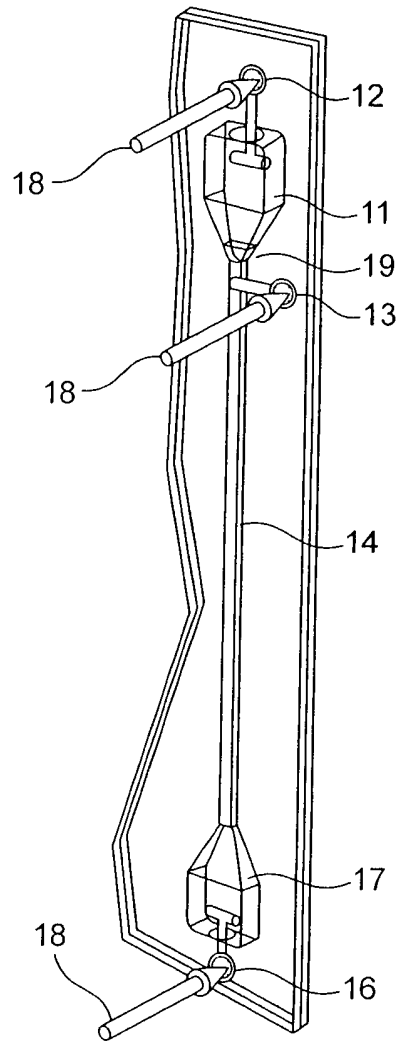


FIG. 18

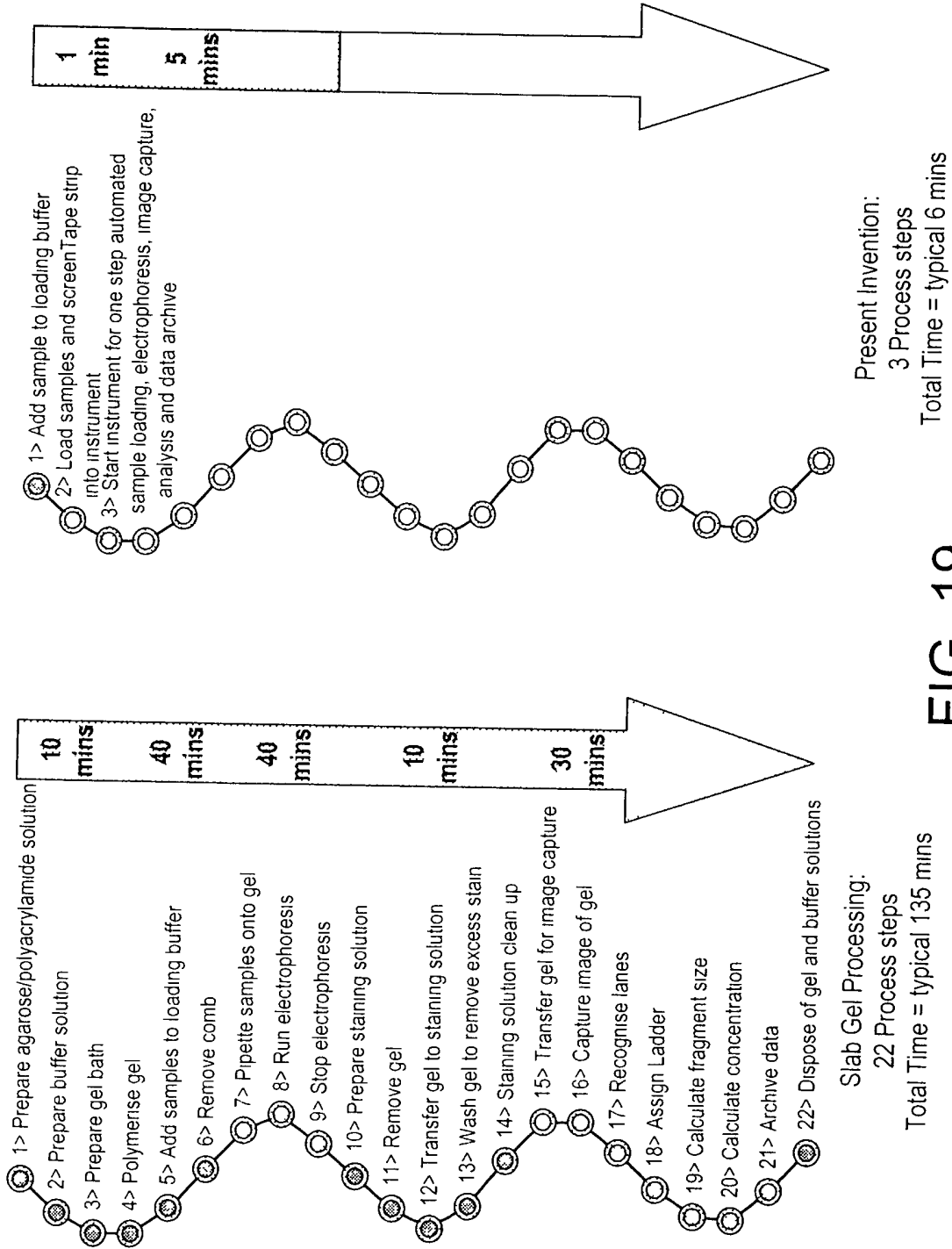


FIG. 19



1 Analysis Instrument

2

3 The present invention relates to an analysis instrument  
4 for use in the determination of properties of biological  
5 and/or biochemical samples using a variety of techniques  
6 including immunoassay, cell based assay and PCR. In  
7 particular, the invention relates to the analysis of  
8 samples containing RNA, DNA or proteins using an  
9 electrophoresis process.

10

11 There are a large number of analysis instruments and  
12 equipment available. Analysis of biological samples  
13 continues to be extensively done on a macro scale and  
14 frequently requires a large number of process steps.

15

16 One of the most extensively used analysis techniques  
17 within the life sciences laboratory is gel bath based  
18 electrophoresis. This process enables separation of a  
19 complex mixture of charged molecules, such as nucleic  
20 acids or proteins, according to their electro-phoretic  
21 mobility. Following this method, the relative molecular  
22 weight and amounts of the constituent molecules can be  
23 determined. However, this well established technique is  
24 time consuming, labour intensive and requires significant  
25 amounts of bench space. Sample preparation, sample  
26 analysis and sample clean-up all involve wet chemistry in  
27 which some of the reagents used (e.g. ethidium bromide)  
28 are toxic, and require specialised handling and disposal  
29 methods.

30

31 A common operating configuration for the electrophoresis  
32 and analysis of DNA fragments using a slab gel includes:

1 an ultra pure demineralised water supply;  
2 bulk supply bottles of buffer reagent;  
3 chemical stains or dyes;  
4 gel powder;  
5 laboratory glassware for gel preparation;  
6 a heating and stirring device for gel preparation (mix  
7 powder with buffer);  
8 a gel tank and all its accessory parts;  
9 an electrical power supply unit;  
10 a sample loading pipette;  
11 a light box on to which the processed gel is transferred  
12 such that the fluorochromes in the gel can be activated;  
13 and  
14 a gel camera, the most basic arrangement of which would  
15 be an instant camera attached to a metal hood which can  
16 be fitted in a light tight arrangement to the light box.  
17  
18 Available improvements to this traditional process are:  
19 pre-cast gels that "drop-in" to a standard gel tank, such  
20 as those provided by the Novex® brand of Invitrogen  
21 Corporation, or the ReadyAgarose® brand of Bio-Rad  
22 Laboratories. However, these gels still require "wet  
23 chemistry" handling procedures and remain time and labour  
24 intensive.  
25  
26 Other improvements include:  
27 rigid gel plates into which the user can cast a gel  
28 matrix;  
29 gel tanks that can simultaneously process multiple pre-  
30 cast or home made gels but which require much handling  
31 and wet chemistry preparation;

1 pre-cast gels that do not require a gel tank or buffers  
2 such as the "E-gel™" system provided by Invitrogen  
3 Corporation (ref US Patents 5,582,702 and 5,865,924).

4

5 The E-gel™ system still incurs the inconvenience and  
6 handling overheads of manual sample loading and the use  
7 of a separate image capture station for analysis

8

9 One of the commonest nucleic acid stainers employed  
10 during electrophoretic separation and imaging is ethidium  
11 bromide. This stainer has the disadvantage of requiring  
12 an Ultra-Violet (UV) light source to trigger the  
13 fluorescence upon which electrophoretic imaging relies. A  
14 requirement of UV imaging systems is to protect the user  
15 from UV radiation using either fully enclosed shielded  
16 light boxes or using goggles within a dark room.

17

18 An arrangement in common use is to use one of a number of  
19 commercially available gel imaging systems. A gel is  
20 processed in the traditional manner in a gel bath, but it  
21 is then manually transferred from the gel bath to the top  
22 surface of a separate light box contained within a light  
23 tight enclosure that contains a digital camera connected  
24 externally by cable to a viewer or an image printing  
25 device. Examples of available systems are manufactured by  
26 UVP Incorporated (brand name *GelDoc-It*), Bio-Rad  
27 Laboratories (brand name *Gel Doc*) or Synoptics Limited  
28 (brand name *Syngene*).

29

30 A similar solution is to use a walk-in dark room which  
31 hosts a UV light box and a camera. However, systems  
32 including these imaging techniques, still require  
33 significant levels of reagent preparation, careful manual

1 sample loading and the set up and use of multiple pieces  
2 of apparatus.

3

4 Examples of systems which automate the traditional slab  
5 gel process are Helena Bio-Sciences, US patents 4,954,237  
6 and 5,147,522. These systems are relatively bulky and  
7 their automation process still involves the preparation,  
8 processing and automated handling of a traditional wet  
9 chemistry slab gel.

10

11 Fully automated electrophoresis devices that use  
12 capillary electrophoresis (as distinct from slab gel  
13 electrophoresis) address some of the issues involved in  
14 gel bath electrophoresis. However, these types of  
15 apparatus are large and expensive and require specially  
16 trained operators. They are normally used to carry out  
17 high resolution separation (down to a single base pair)  
18 of nucleic acids or high throughput single nucleotide  
19 polymorphism (SNP) analysis where automation is  
20 essential. An example of this type of system is the  
21 Applied Biosystems Inc Prism 3100 Genetic Analyser.  
22 The cost and complexity of these systems usually  
23 prohibits their use in small laboratories.

24

25 Microfluidic devices are beginning to be used in  
26 molecular biology. The Agilent Bio-analyser 2100 is a  
27 bench top device using the Caliper "Labchip®". This  
28 system exploits microfluidic techniques to achieve rapid  
29 separation. The system is however not fully automated  
30 and samples are processed in a serial (as opposed to  
31 parallel) fashion.

32

1 The challenges for systems that seek to replace slab gel  
2 electrophoresis and aim to achieve significant reductions  
3 in separation time are:

4 to eliminate the need for reagent preparation (gel,  
5 buffer, electrolyte) other than those associated with  
6 test sample preparation.

7

8 In addition, a number of challenges exist in the general  
9 field of analysing biological and or biochemical samples  
10 such as:

11 to allow the user to load samples in a range of different  
12 standard laboratory vessel types;

13 to employ a micro-scale separation device to speed up  
14 molecule separation without the risk of joule heating;

15 to achieve highly parallel testing leading to improved  
16 sample throughput;

17 to reduce the quantities (therefore the cost) of reagents  
18 and test samples used;

19 to automate the process such that process steps are  
20 integrated and user intervention is minimised;

21 to achieve these improvements using a very small  
22 footprint;

23 to achieve all of the above in a manner which is cost  
24 competitive with traditional slab gel processing.

25

26 It is the object of the present invention to provide an  
27 analysis instrument in which the above challenges are  
28 addressed and whereby samples are analysed in a quick,  
29 clean and efficient manner.

30

31 In accordance with a first aspect of the present  
32 invention, there is provided an analysis instrument for  
33 processing a microfluidic device, comprising sample

1 storage means, a microfluidic device holder, sample  
2 loading means for loading sample into a microfluidic  
3 device disposed in the holder, processing means for  
4 enabling a reaction in a microfluidic device, and  
5 detection means for detecting and/or measuring the  
6 reaction, characterised in that the microfluidic device  
7 holder is adapted to hold the microfluidic device  
8 comprising or including a tape in position for processing  
9 and/or detection.

10

11 The reaction carried out in the microfluidic device may  
12 be electro-chemical and/or bio-chemical.

13

14 Preferably, the sample loading means is moveable relative  
15 to the sample storage means and relative to the  
16 microfluidic device holder.

17

18 The instrument may further comprise opening means for  
19 opening a microfluidic device.

20

21 Preferably, the sample loading means and the microfluidic  
22 device opening means are disposed a fixed distance apart  
23 on a moveable common support and spaced such that the  
24 sample loading means can acquire sample from the sample  
25 storage means whilst at the same time the microfluidic  
26 device opening means opens the microfluidic device.

27

28 The sample loading means may comprise a nozzle, the  
29 nozzle being adapted to removably mount a pipette tip,  
30 the nozzle further being operably attached to a pump for  
31 pumping liquid into a mounted pipette tip.

32

1 Alternatively, the sample loading means comprises a pump,  
2 which can aspirate liquid from the sample storage means  
3 and dispense liquid into the microfluidic device.

4 Preferably, the pump has a pump nozzle, the pump nozzle  
5 being attachable to a pipette tip.

6

7 Preferably the pump and the microfluidic device opening  
8 means are mounted to a common support structure and they  
9 are spaced a fixed distance apart such that the pump can  
10 acquire a new sample at the same time as the microfluidic  
11 device opening means prepares the microfluidic device for  
12 receiving that new sample.

13

14 Optionally the pump and the microfluidic device opening  
15 means are mounted to a common support structure and they  
16 are spaced a fixed distance apart such that the pump can  
17 pick up a pipette tip at the same time as the  
18 microfluidic device opening means prepares the  
19 microfluidic device for receiving that new sample.

20

21 The instrument may further include means for removal of a  
22 used pipette tip from the nozzle. The removal means may  
23 comprise a flange, the pipette tip being removed by  
24 relative movement between the mounted pipette tip and the  
25 flange. Preferably, the instrument includes a receptacle  
26 for receiving a spent pipette tip.

27

28 Preferably, the instrument includes a fresh pipette tip  
29 store adapted to store pipette tips such that the nozzle  
30 can be brought into contact with a pipette tip for  
31 attachment to the nozzle. In this embodiment, the  
32 receptacle and the store are preferably parts of a single  
33 demountable unit.

1

2 Preferably, the microfluidic device opening means  
3 comprises a piercing tool for penetrating a membrane of  
4 the microfluidic device. The piercing tool may be  
5 removably mounted on the moveable common support, and  
6 said piercing tool may comprise a needle.

7

8 Preferably, the needle has a shaped point that can cut an  
9 opening in the microfluidic device in the form of a flap  
10 that remains joined to the device.

11

12 The instrument may include means for removal of a used  
13 needle from the moveable common support.

14

15 Preferably, the removal means comprises a flange, the  
16 used needle being removed by relative movement between  
17 the needle and the flange. The instrument preferably  
18 includes a receptacle for receiving a used needle.

19

20 Preferably, the analysis instrument comprises an  
21 automatic needle changeover means, in the event that the  
22 needle becomes blunt through usage.

23

24 Preferably the needle comprises a means of automatic  
25 attachment to the automatic needle changeover means.

26

27 This enables rapid attachment and removal without the use  
28 of any tools and without the need for user intervention.

29

30 Preferably, the automatic needle changeover means  
31 comprises a cartridge containing a receptacle to receive  
32 the used needle and a receptacle containing a new needle.

33



1 Preferably, the cartridge is automatically loadable into  
2 the automatic needle changeover means in the instrument.  
3 This eliminates a hazard as a user prevented from  
4 handling both the old and the new needles.

5

6 Preferably the cartridge can be automatically drawn into  
7 the analysis instrument under the control of machine  
8 software.

9

10 Preferably a needle attachment means, the needle  
11 cartridge and the motion system of the analysis  
12 instrument can cooperate to achieve automated needle  
13 changeover.

14

15 Preferably, the instrument is adapted to maintain a count  
16 of needle usage to alert a user to a requirement for  
17 needle changeover.

18

19 Preferably this process is aided by the instrument  
20 control software which will maintain a count of needle  
21 usage (number of piercings) such that the external  
22 personal computer can alert the user to a requirement for  
23 needle changeover. Accordingly, the potential  
24 disadvantage of the needle becoming blunt is overcome.

25

26 The instrument may include a fresh needle store adapted  
27 to store needles such that the common support can be  
28 brought into contact with a needle for attachment  
29 thereto. Preferably, the receptacle and the store are  
30 parts of a single demountable unit.

31

32 Preferably, the sample storage means comprises a sample  
33 holder, which can accommodate one or more standard

1 laboratory vials or a standard laboratory multi-well  
2 plate.

3

4 The instrument may be operable to process a single sample  
5 using one single element of a microfluidic device.

6

7 Alternatively, the instrument may be operable to process  
8 a single sample using one single element of a  
9 microfluidic device by comprising a single sample loading  
10 means only, the single sample loading means being enabled  
11 to load sample one sample at a time from a plurality of  
12 sample holders, and deliver each said sample to a  
13 separate element of a microfluidic device.

14

15 Preferably, the instrument is operable to permit a batch  
16 of multiple samples to be processed up to the limit of  
17 the test element capacity of a single microfluidic  
18 device.

19

20 Alternatively, the instrument is operable to permit a  
21 batch of multiple samples to be processed up to the limit  
22 of the capacity of a microfluidic device feeder module.

23

24 Thus, the system has the flexibility to cope with a range  
25 of samples from one to many.

26

27 Preferably, the sample storage means includes a pipette  
28 tip holder, which may be a used pipette tip holder.

29

30 Preferably the pump includes means for removably  
31 attaching a pipette tip to the pump.

32

1 The pump must be configured to pick up a pipette tip for  
2 one time use in the handling of a sample. In addition,  
3 the pump can dispose of a used pipette tip once the  
4 sample is loaded into the microfluidic device.

5

6 Preferably, the used pipette tip holder is provided with  
7 removal means for removing the pipette tip from the pump.

8

9 Preferably, the removal means is provided with an opening  
10 shaped to catch a used pipette tip so that it is retained  
11 in the used pipette tip holder when the pump is  
12 retracted.

13

14 Preferably, the sample loading means is moveable to  
15 ensure the used pipette tip is caught upon the opening of  
16 the used pipette holder.

17

18 Optionally, the sample storage means is mounted on a  
19 platform, moveable relative to the sample detection  
20 means.

21

22 Preferably, the sample detection means and the  
23 microfluidic device holder are moveable relative to one  
24 another to allow samples within the microfluidic device  
25 to be positioned at a predetermined location for  
26 detection.

27

28 Preferably, the microfluidic device holder is adapted to  
29 accommodate a microfluidic device having a plurality of  
30 microfluidic processing elements such that each said  
31 element can be individually detected by the detection  
32 means.

33

1 Preferably, the microfluidic device holder is mounted on  
2 the same platform as the sample storage means.

3

4 Preferably, the microfluidic device holder has one or  
5 more aperture to allow the reaction in the sample to be  
6 monitored.

7

8 Optionally, the sample processing equipment holder is  
9 provided with a reflective surface adjacent to the  
10 position in which microfluidic processing apparatus is  
11 mountable.

12

13 Preferably, the processing means is adapted to facilitate  
14 bio-molecular separation.

15

16 Preferably, the sample processing means comprises probes  
17 for applying voltages to a sample, the probes being  
18 configured in an array to correspond with an equivalent  
19 array of conductive pads on the microfluidic device.

20

21 Preferably, the electrical polarity of the probes is  
22 controllable.

23

24 Optionally, the processing means can comprise any  
25 combination of

26 sample preparation including fractionation, isolation or  
27 purification

28 polymerase chain reaction

29 bio-molecular separation

30 molecular binding by affinity

31 isolation of any reaction end products

32 retrieval of any reaction end products.

33

1

2 Optionally, the microfluidic device within the  
3 microfluidic device holder can be indexed past a fixed  
4 detection point so that one or more test elements can be  
5 monitored for the results of any reaction process. Test  
6 elements may be monitored simultaneously.

7

8 Preferably, the sample loading means is mounted on a  
9 frame above the sample storage means for movement to and  
10 from the sample storage means and in a direction  
11 substantially perpendicular to the movement direction of  
12 the sample storage means.

13

14 Optionally, the sample processing means comprises a  
15 plurality of probes for applying voltage to a sample in a  
16 microfluidic device mounted in the holder. The probes may  
17 be disposed to contact conductive pads of the  
18 microfluidic device. The instrument may be adapted to  
19 enable electro-phoretic separation of a sample  
20 containing, molecules of DNA or RNA or proteins.

21

22 Optionally, the instrument may be adapted to enable  
23 electro-kinetic transport of a biological sample past a  
24 zone within the microfluidic device that contains one or  
25 more antibodies, such that binding between the sample and  
26 any antibody material can be enabled.

27

28 Preferably, the detection means is adapted to detect  
29 change in conductivity in a sample.

30

31 Optionally, the detection means can be electro-chemical,  
32 whose function is enabled by electrical probes in contact  
33 with the microfluidic device such that any change in

1 conductivity from a sample reaction process can be  
2 detected.

3

4 Preferably, the sample detection means comprises an  
5 optical assembly.

6

7 Preferably, the optical assembly includes a light source  
8 for exciting a sample in a microfluidic device holder and  
9 a receiver arranged to receive a signal from said  
10 microfluidic device holder, the receiver being arranged  
11 in an optical path relative to the microfluidic device  
12 holder.

13

14 Preferably, the optical assembly includes a light source  
15 capable of emitting at a predetermined first frequency  
16 for excitation of constituents of the sample to allow the  
17 sample to emit light at a second frequency, and a light  
18 receiver. The receiver may comprise a charged coupled  
19 device, or a line scan camera. The receiver may be  
20 configured to send image data to an external data  
21 processing device.

22

23 Preferably, the receiver comprises a charged coupled  
24 device.

25

26 Alternatively, the receiver is a line scan camera.

27

28 Preferably, the light source and receiver are on the same  
29 side of the Microfluidic device holder.

30

31 Optionally, the light source and receiver are on opposing  
32 sides of the microfluidic device holder.

33

1 Optionally, the light source projects directly into the  
2 light path of the optical assembly.

3

4 Optionally, the light source emits in the ultra-violet  
5 range of the electromagnetic spectrum.

6

7 Preferably, the receiver is capable of detecting light in  
8 the visible range of the electromagnetic spectrum.

9

10 Preferably, the receiver can be configured to send image  
11 data to an external data processing device.

12

13 Preferably, the data processing device is a Personal  
14 Computer.

15

16 Optionally, the data processing device, which may be a  
17 Personal Computer, can be embodied within the analysis  
18 instrument.

19

20 Preferably, the system control of the analysis instrument  
21 is hosted on that same personal computer.

22

23 The instrument may include an on-board system controller,  
24 the controller being programmable by a user to perform  
25 automated microfluidic device processing, or, as an  
26 alternative, the instrument may be adapted to be  
27 controlled by an external system controller.

28

29 Preferably, the analysis instrument is configured to  
30 operate from low voltage electrical supplies and that an  
31 external dc power supply, such as is used by a laptop  
32 computer, can be its primary source of electrical supply.

33

1 The system can be modularly extended to incorporate  
2 automated handling of multiple microfluidic devices, for  
3 example, to allow continuous processing of a micro-titre  
4 plate and/or automated handling of pipette tips and/or  
5 automated handling and storage of used microfluidic  
6 devices.

7

8 Preferably, the automated handling is provided by a  
9 feeder module removeably attachable to the analysis  
10 instrument and that this module can store multiple  
11 microfluidic devices that can be automatically loaded  
12 into or unloaded from the microfluidic device holder.

13

14 One benefit of the invention described herein over the  
15 current state of the art is that it integrates a novel  
16 microfluidic device with a novel analysis instrument  
17 possessing an adaptable handling configuration. The  
18 resulting system is very easy to use and can achieve high  
19 test throughput within an extremely small footprint.

20

21 The sample loading mechanism can use a consumable  
22 laboratory pipette tip which eliminates the risk of  
23 contamination from previously processed samples, includes  
24 a means of storing and disposing of tips, and optionally  
25 allows the sample loading pipette to be washed at a wash  
26 station within the apparatus.

27

28 The instrument may include a feeder module removeably  
29 attachable to the instrument and storing multiple  
30 microfluidic devices for automatic loading into or  
31 unloading from the microfluidic device holder.

32



1 The sample loading mechanism can use a consumable  
2 laboratory pipette tip which eliminates the risk of  
3 contamination from previously processed samples, includes  
4 a means of storing and disposing of tips, and optionally  
5 allows the sample loading pipette to be washed at a wash  
6 station within the apparatus.

7

8 In accordance with a second aspect of the invention there  
9 is provided a microfluidic processing device, comprising  
10 a reaction chamber, a sample loading chamber into which a  
11 sample is injectable, the reaction chamber being  
12 operatively connected to the sample loading chamber, a  
13 cover that extends across at least part of the sample  
14 loading chamber, the cover and the reaction chamber  
15 comprising pierceable material and being separated by an  
16 overspill cavity configured to accept any overspill of an  
17 injected sample.

18

19 Preferably, the reaction chamber contains a molecular  
20 separation medium.

21

22 The reaction chamber may be a channel and the  
23 microfluidic processing device may further include a  
24 receiving chamber at an end of the reaction channel  
25 remote from the sample loading chamber.

26 The microfluidic device may be used with the analysis  
27 instrument of the first aspect of the invention.

28

29 The presence of the overspill cavity allows excess  
30 reagent that would otherwise be spilled into the analysis  
31 instrument to be contained between the cover and the  
32 loading chamber.

33

1

2 Preferably, the cover and/or the loading chamber are  
3 manufactured from polymer film.

4 Preferably, the microfluidic processing device further  
5 comprises electrodes.

6

7 The chambers and electrodes of a single microfluidic  
8 element combine to become a single processing element.

9 Preferably, a single processing element is provided with  
10 three electrical contacts.

11

12 Preferably, the three electrical contacts operate as a  
13 cathode, a compacting electrode and an anode.

14

15 Preferably, the cathode is arranged in the loading  
16 chamber, the compacting electrode is arranged at the  
17 upper end of the reaction channel and the anode in the  
18 receiving chamber.

19

20 The polarities of the electrical contacts may be  
21 reversed.

22

23 Preferably, the electrical contacts extend from a  
24 position outside the microfluidic device to a position  
25 inside the microfluidic device.

26

27 Preferably, the electrical contacts have coupling means  
28 for connecting them to an external electrical supply to  
29 allow the creation of a circuit incorporating the  
30 reaction chamber.

31

1 Preferably, reagents within the microfluidic device are  
2 pre-filled at the point of manufacture, thereby avoiding  
3 the need for reagent handling at the point of use.

4

5 Preferably, the loading chamber is pre-filled with an  
6 electrolyte.

7

8 Preferably, the reaction channel is pre-filled with a  
9 molecular separation medium.

10

11 Preferably, the receiving pocket is pre-filled with  
12 either the molecular separation medium or an electrolytic  
13 buffer.

14

15 The microfluidic processing device may have a laminated  
16 structure.

17

18 Preferably, the microfluidic processing device includes  
19 optical fiducial marks whose position is known relative  
20 to the reaction chamber and which can be acquired by the  
21 detection means of an analysis instrument to accurately  
22 identify the position of a reaction process.

23 microfluidic device holder.

24

25 Preferably the device further comprises an identifying  
26 label or tab.

27

28 Preferably this tab can be used as a handling tab for  
29 loading and unloading the microfluidic device such that  
30 manual contact with any optical surface of the device is  
31 avoided.

32

1 According to a third aspect of the invention there is  
2 provided a kit comprising an instrument as hereinbefore  
3 defined, and a microfluidic device as herein defined.

4

5 One benefit of the invention described herein over the  
6 current state of the art is that it integrates a novel  
7 microfluidic device with a novel analysis instrument  
8 possessing an adaptable handling configuration. The  
9 resulting system is very easy to use and can achieve high  
10 test throughput within an extremely small footprint.

11

12 The present invention will now be described by way of  
13 example only with reference to the accompanying drawings  
14 in which:

15

16 Figure 1 shows a general external view of the processing  
17 instrument for a microfluidic device;

18

19 Figure 2 shows the zones of the instrument that an  
20 operator will access for loading the system;

21

22 Figure 3a is a side view of an embodiment of the present  
23 invention and Figure 3b is a corresponding plan view;

24

25 Figures 4a to 4G show the automated handling sequence for  
26 a test sample;

27

28 Figure 5a shows how test samples can be loaded from open  
29 topped laboratory vials;

30

31 Figure 5b shows how test samples can be loaded from  
32 laboratory vials with a hinged lid;

33

1 Figure 5c shows how test samples can be loaded from a  
2 multi well plate;

3

4 Figures 6a and 6b show an arrangement for retaining the  
5 pipette tip holder within the instrument;

6

7 Figures 6c and 6d show the use of the same arrangement as  
8 in figures 6a and 6b to retain a needle cartridge whereby  
9 the piercing tool for the microfluidic device can be  
10 automatically replaced;

11

12 Figure 7 shows the instrument enclosure configured to  
13 accommodate an automatic feeder module for microfluidic  
14 devices;

15

16 Figure 8 shows a more detailed side view of the feeder  
17 module configuration;

18

19 Figure 9 is a plan view of the base section of an  
20 alternative embodiment of an analysis instrument in  
21 accordance with the present invention;

22

23 Figure 10 is a side view of the analysis instrument of  
24 Figure 9;

25

26 Figure 11 is a plan view of a microfluidic processing  
27 device with eight separate microfluidic processing areas;

28

29 Figure 12 is a plan view of a microfluidic processing  
30 device with sixteen separate microfluidic processing  
31 areas;

32

1 Figure 13 is a side view of the microfluidic device  
2 holder of the embodiment of the present invention shown  
3 in Figures 9 and 10;

4

5 Figure 14 shows quadrant markers and areas of interest  
6 found on the microfluidic processing apparatus used in  
7 the analysis instrument of the present invention;

8

9 Figure 15 is a side view of a probe block as used in the  
10 embodiment of Figure 9 and 10 of the present invention;

11

12 Figure 16 shows details of the upper part of a single  
13 test element of the microfluidic device in accordance  
14 with the second aspect of the invention;

15

16 Figure 17a shows how the microfluidic device is loaded  
17 with a test sample;

18

19 Figure 17b shows further detail of the method of piercing  
20 the microfluidic device and the method of containment of  
21 any spillage.

22

23 Figure 18 shows one complete segment of the microfluidic  
24 device including illustration of the method of  
25 interfacing the external probes; and

26

27 Figure 19 shows a comparison of slab gel processing and  
28 processing using an embodiment of the present invention.

29

30 Figure 1 shows a typical instrument enclosure. A main  
31 enclosure component 60 carries a lid 61 at the front for  
32 operator access to the loading and unloading stations and

1 a rear cover 62 for access to the onboard drive and  
2 control circuit boards.

3

4 Figure 2 shows the operator loading stations. Station 63  
5 is the sample loading and unloading station, station 64  
6 is the pipette tip loading and unloading station, station  
7 65 is the microfluidic device loading and unloading  
8 station.

9

10 Figures 3a and 3b show a microfluidic device 1 held  
11 within holder 21 which is mounted to platform 27 which is  
12 movable in one axis along slides 28. These slides are  
13 attached to baseplate 38. Also mounted to platform 27 is  
14 the electrical probe block assembly 22, a pipette tip  
15 holder 23 which can store unused pipette tips 24 and used  
16 pipette tips 25. A suitable pipette tip is, for example,  
17 the "Eppendorf PMP-885-501W" and a typical sample loading  
18 volume is around 1 microlitre, but conveniently could be  
19 in the range 0.1 to 5 mcrolitres. Also mounted on this  
20 platform is the test sample storage device, in this case  
21 a 96 well micro-titer plate 26. Nothing precludes other  
22 types of micro-titer plate (e.g. 384 well) or even the  
23 use of individual vials for sample storage.

24

25 Above the movable platform 27 is a fixed gantry beam 36  
26 supported by pillars 37 on the baseplate 38. Baseplate  
27 38, in turn, is attached to lower casing 39. A slide 35,  
28 along which a carriage plate 34 can move is attached to  
29 the gantry 36. This movement is transverse to the  
30 movement of platform 27.

31

32 A vertical slide 33 along which carriage plate 31 can  
33 move is attached to carriage plate 34. A pump 30 and an

1 arm 32 which locates a piercing tool 40 is attached to  
2 carriage plate 31.

3

4 Baseplate 38 also supports the image capture assembly 41  
5 which comprises a CCD camera 42, a lens 43, a filter 44,  
6 a mirror (or prism) 45, a lampholder 46 which contains  
7 lamp tubes 47, reflectors 48, lenses 49 and a slit 50  
8 through which the camera light path can pass.

9

10 Control for the various active functions of the  
11 instrument and delivery of the captured images is  
12 provided by electronic controller 51, which comprises a  
13 micro-controller whose programme sequence is delivered  
14 from an external personal computer via, for example, a  
15 USB cable. The particular architecture allows the  
16 instrument enclosure to be serviced by only two cables,  
17 one for delivery of DC power, the other a communications  
18 cable to the external PC. This layout contributes to the  
19 extremely compact footprint of the instrument enclosure.

20

21 Figures 3a and 3b also show the pump 30 positioned ready  
22 to withdraw test sample from the first well of the second  
23 row of the micro-titer plate 26. This is achieved by  
24 suitably synchronizing the positions of platform 27,  
25 carriage 34 and carriage 31 which are controlled as  
26 elements of a 3-axis Cartesian robot. The drives and  
27 controls for this X, Y, Z system are not described since  
28 the means of achieving this are already known, but, for  
29 example, the drives can be lead screws driven by stepper  
30 motors and the control can be from a software sequence  
31 embedded in a micro-controller.

32



1 Figures 4a to 4g show a "snapshot" of the processing  
2 sequence whereby platform 27 has moved from the operator  
3 load station 51 into the sample transfer station. This  
4 station is behind bulkhead 52 so that load station 51 is  
5 isolated from the internal mechanisms of the instrument.

6

7 An advantageous step in this sequence is that the  
8 piercing tool 40 opens an access port in the microfluidic  
9 device 1 by means of penetration of pocket 7 and cavity  
10 11 and that it does this simultaneously with the pick up  
11 of pipette tip 24.

12

13 Figures 5a to 5c show arrangements that allow the user  
14 to load test samples either in individual vials 20 or in  
15 a strip of vials (for example, a PCR strip) or in a  
16 multi-well plate 26, which can be a 96 well micro-titre  
17 plate or a 96 well PCR thermo-cycler plate. These vials  
18 and plates are mounted on a common support block 29.  
19 This arrangement is also compatible with other types of  
20 micro-titre plate, for example, a 384 well plate. Figure  
21 5b shows the use of a vial 201 with hinged lid 202. The  
22 lid is trapped under the lid retaining plate 203, that  
23 has an access aperture 204.

24

25 Figure 6a shows an arrangement that allows pipette tips  
26 24 to be loaded in a removable pipette tip holder 23  
27 which can be securely retained within support block 160  
28 by a latch mechanism 161 which engages the tongue 162 of  
29 a pivotable lever 163 into an undercut feature 164 on the  
30 underside of pipette tip holder 23. The pipette tip  
31 holder 23 incorporates a slotted flange 165 which allows  
32 a used tip to be entered into the pipette tip holder 23  
33 such that a small sideways motion of the pipette tip 25

1 engages the pipette tip with the underside of the slotted  
2 flange 165 and such that when the pump nozzle holding the  
3 pipette tip is retracted vertically upwards, the used  
4 pipette tip is disengaged to fall into the pipette tip  
5 holder. The latch mechanism 161 ensures that the pipette  
6 tip holder 23 is not withdrawn during this operation.  
7 Figure 6b shows the latch mechanism 161 disengaged to  
8 allow the operator to remove and replace the pipette tip  
9 holder in the direction of arrow "A".

10

11 Figure 6c shows how this same arrangement can be used to  
12 allow automated replacement of the piercing tool for the  
13 microfluidic device, this piercing tool comprising a  
14 needle 167. A needle cartridge 166 (instead of the  
15 pipette tip holder 23) contains a new needle 167 and  
16 space to accommodate the used needle 168. The cartridge  
17 may have a peel-off or removable lid to expose the new  
18 needle. The new needle can be retained temporarily during  
19 the loading process by a foam plug 170. Needle  
20 replacement involves a motion sequence of the needle  
21 holder 169 which is mounted on, for example, arm 32 of  
22 figure 3a. With further reference to figure 3a it can be  
23 seen that the motion system capable of manipulating pump  
24 30 is equally capable of manipulating needle 167 as part  
25 of an automated replacement sequence. With reference to  
26 Figure 6d, the needle holder 169 enters the used needle  
27 168 into a cavity of the needle cartridge 166 which  
28 incorporates a similar slotted flange 165 to that used in  
29 pipette tip holder 23, thereby enabling removal of the  
30 used needle. The needle holder 166 is prevented from  
31 withdrawal by the retaining action of latch mechanism  
32 161. Thus the holder 160 and latch mechanism 161 can  
33 serve an important dual function, that is, retention of a

1 pipette tip holder during normal use or retention of a  
2 needle cartridge during the maintenance sequence for  
3 replacing the piercing tool. The needle replacement  
4 sequence can be initiated by the system storing a count  
5 of the number of piercings carried out (for example in  
6 EEPROM) and alerting the operator on the system PC once a  
7 preset count is reached.

8

9 Figure 7 shows the integration of a separate discrete  
10 feeder module 66 whose function is to allow multiple  
11 microfluidic devices to be automatically loaded and  
12 discarded. Used microfluidic devices are disposed of  
13 into a drawer 67 which can be opened for emptying. This  
14 configuration is targeted at providing "hands off"  
15 operation for automated processing of one complete multi-  
16 well plate of test samples.

17

18 Figure 8 shows details of the feeder mechanism. A  
19 loading hopper 70 can stack multiple microfluidic devices  
20 1. These devices are held together by a spring loaded  
21 paddle 71 which pushes the stack of microfluidic devices  
22 1 against a restraining lip 73 which extends up each side  
23 and along the bottom edge of the microfluidic device at  
24 the front of the stack. Paddle 71 mounts to a slide  
25 which is attached to support plate 72. Surrounding the  
26 hopper area is a frame comprising side plates 74 and a  
27 cross plate 75. This frame is attached to support plate  
28 72. The side plates 74 incorporate slides 76 which carry  
29 a cross beam 77 which carries a vertical slide 78 to  
30 which is mounted a pick up tool 79. This tool can be  
31 positioned by means of suitable linear actuator drives  
32 (not shown) such that at position 79a it can pick a  
33 microfluidic device from the front of the hopper stack

1 70, at position 79b it can load the microfluidic device  
2 into the holder 21, at position 79c it can deposit the  
3 used tape into the waste trap 80 which is integrated with  
4 drawer 67.

5

6 The remaining requirement for fully automated handling is  
7 to provide automated pipette tip handling. This can be  
8 accomplished by the pick and place unit 84 which will  
9 load pipette tips from a standard pipette holding tray  
10 into the tip holder 23.

11

12 The alternative is to replace tip holder 23 with a wash  
13 bath 82. The liquid transfer pump 30 will be fed with a  
14 wash compound and pump fresh washing agent through the  
15 liquid transfer nozzle into wash bath 82 which will  
16 overspill into catchment tray 83, which will drain into a  
17 sump container underneath the test sample loading zone.

18

19 Figure 9, shows an alternative embodiment of the analysis  
20 instrument of the present invention. The base area 102 of  
21 the analysis instrument is shown in plan and comprises a  
22 sample assembly 103 having a sample assembly platform 105  
23 upon which a cartridge holder 107 and a tape holder 115  
24 are mounted. The cartridge holder 107 contains a pipette  
25 tip holder 109, a used pipette tip holder 111 and a  
26 sample chamber 113. The sample to be analysed is kept in  
27 chamber 113 and the pipette tips are kept in pipette tip  
28 holder 109 prior to their use.

29

30 The used pipette tip holder 111 has a keyed shape. That  
31 is, the entrance to the pipette tip holder is narrowed  
32 towards one end of it. This narrowing allows the edge of  
33 a pipette tip to be caught on the narrowed section of the

1 used pipette tip holder and assists in the removal of the  
2 pipette tip from the pump nozzle 147 (Figure 10). It  
3 should be noted that the cartridge holder 107  
4 accommodates eight pipette tip holders 109, used pipette  
5 tip holders 111 and sample chambers 113. This size of  
6 cartridge holder 107 has been chosen for convenience and  
7 it is anticipated that a cartridge holder with space for  
8 more than or less than eight samples could be used.

9

10 The tape holder 115 consists of a box shaped section  
11 having one open side 157 (Figure 13) and an open top end  
12 116 into which a microfluidic processing apparatus can be  
13 inserted.

14

15 The analysis instrument is designed such that each of the  
16 microfluidic processing channels is substantially in  
17 alignment with the corresponding sample chamber 113.  
18 Consequently, the microfluidic processing tape as used  
19 with this embodiment of the present invention will  
20 contain eight separate microfluidic processing areas.  
21 Platform 5 is mounted on rails that allow it to move to  
22 and from the position of the probe block 133.

23

24 The optical assembly 117 consists of a platform 118 which  
25 allows the entire assembly to move in direction B. A  
26 camera 119 is provided with a lens 121 and a prism 123  
27 which is used to redirect a beam of light that has been  
28 reflected from the sample when in use. The prism is  
29 partially enclosed within an opaque enclosure 125 which  
30 also partially encloses two radiation sources 129. In  
31 this example, these sources emit ultra-violet radiation  
32 at a wavelength of approximately 310 nm. It will be  
33 appreciated that, depending upon the analysis undertaken,

1 radiation sources emitting radiation at other wavelengths  
2 may be used. The radiation sources are provided with a  
3 transparent screen 127 that allows radiation to pass out  
4 from the opaque enclosure 125 towards the probe block 131  
5 where analysis of the sample is undertaken.

6  
7 The probe block 131 in this example contains a number of  
8 pins 135. As can be seen from Figure 15, these pins are  
9 arranged such that two pins in each row are positioned  
10 towards the top of the probe block and a single pin is  
11 positioned towards the bottom. The polarity of each of  
12 the pins may be changed to enhance analysis of the sample.

13  
14 Figure 10 shows the side view of the embodiment of the  
15 analysis instrument of Figure 9. In this diagram the  
16 optical assembly 117, the cartridge holder 107 and the  
17 tape holder 115 are shown as described above.

18  
19 In addition, a sample transfer means is shown. The  
20 sample transfer means consists of a tape filler having a  
21 pump 145, connected to a pump nozzle 147 that extends  
22 downwards towards the position of the cartridge holder  
23 107. The sample transfer means is further provided with  
24 a tape puncturing means 149 which in this example  
25 comprises a needle with a shaped point that extends down  
26 towards the position of the tape holder 115.

27  
28 These devices are mounted on a moveable frame 41 which  
29 allows movement in directions D and E as shown in Figure  
30 10. In addition, the distance between the pump nozzle  
31 147 and the tape puncturing means 149 is defined by  $x$ .  
32 This distance is substantially identical to the distance

1 between the tape holder 115 and the sample chamber 113,  
2 also denoted by X on Figure 10.

3

4 Figure 13 shows the side view of tape holder 115 and  
5 shows a number of reflective pads 159. In use, these  
6 pads provide a reflective background which lies behind  
7 the position of quadrant markers 155 which are found on a  
8 microfluidic processing device as shown in Figure 14.

9

10 The combination of these reflective pads and the quadrant  
11 markers allows easy alignment of the optical assembly 117  
12 to maximise the amount of reflected radiation that is  
13 detected by the camera 119.

14

15 In use a set of samples is loaded into the sample  
16 chambers 113 and a set of pipette tips are loaded into  
17 the pipette tip holders 109. A microfluidic processing  
18 device such as a microfluidic processing tape, having  
19 eight microfluidic processing areas is then loaded into  
20 the tape holder 115. Thereafter, the moveable frame 141  
21 moves the tape filler 143 into position above the pipette  
22 tip holder 109 and is then lowered in order to pick up a  
23 pipette.

24

25 Thereafter, the tape filler moves to the position above  
26 the sample chamber 113 and is then lowered into a sample  
27 chamber 113 where the pump is actuated and the sample is  
28 drawn into a pipette which is coupled to the pump nozzle  
29 147 of tape filler 143. Substantially simultaneously,  
30 the tape puncturing means 149 is lowered to the tape  
31 holder 115 where the tape puncturing means punctures a  
32 hole in a microfluidic processing area of the

1 microfluidic processor (which in this example is in tape  
2 form).

3

4 Advantageously, therefore, a single processing step  
5 allows a hole to be punctured in the microfluidic  
6 processor and allows a pipette to be filled.

7

8 Thereafter, the pipette on the end of the pump nozzle 47  
9 is moved to a position above the tape holder 15 and  
10 subsequently lowered to allow the microfluidic processing  
11 area to be filled with the sample.

12

13 These process steps are repeated until the samples have  
14 been removed from each of the sample chambers 13 and  
15 added to the corresponding microfluidic processing areas  
16 found in the tape holder 15.

17

18 Turning to Figure 9, once the sample is in the  
19 microfluidic processing area 115, the sample assembly  
20 platform is moved in direction A towards the probe block  
21 131 and the probe block 131 moves towards the tape  
22 holder. The probe block pins move through the open side  
23 157 of the tape holder and are coupled to electrical  
24 connections upon the microfluidic processing areas.

25

26 As can be seen in Figure 15, there are sets of three pins  
27 which are coupled to each microfluidic processing area.

28 The polarity of these pins can be reversed. For  
29 example, in the analysis of DNA, once the negatively  
30 charged DNA sample has been added to the microfluidic  
31 processing area, the polarity of pin 135a is set to  
32 negative and the polarity of pin 135b is set to positive.  
33 This allows the DNA to form a consistent mass at or near



1 the electrode 135b. Thereafter, this electrode is  
2 switched off and electrode 135c is given a positive  
3 polarity so that the DNA sample can migrate down the  
4 column.

5  
6 During this processing, the radiation sources 129 emit  
7 radiation at 310 nm onto the sample. In the case of a  
8 DNA sample such incident radiation provides an output at  
9 600 nm in the visible spectrum. This radiation is  
10 provided to the camera by the total internal reflection  
11 by the prism 23 and the camera detects the lights and  
12 provides results accordingly.

13  
14 Figures 11 and 12 show the outline profile of a  
15 microfluidic device whose configuration is compatible  
16 with the instrument processing methods already described.  
17 The spacing between test elements on the microfluidic  
18 device is conveniently set at the same spacing as the  
19 wells of standard laboratory micro titre plates, for  
20 example, in Figure 11 showing an 8-way microfluidic  
21 device, the spacing between elements is 9mm to correspond  
22 with a 96 well plate. Similarly in Figure 12 showing a  
23 16-way microfluidic device, the spacing between elements  
24 is 4.5mm to correspond with a 384 well plate. Figure 11  
25 also shows locations 12, 13 and 16 which are electrodes  
26 in contact with the reagents inside the device but which  
27 pass between layers of the device such they can be  
28 accessed by external probes 18 of Figure 18.

29  
30 Figures 16 to 18 show further views of a suitable  
31 microfluidic device. For the purpose of example, a three  
32 layer polymer lamination is shown. A transparent layer 2  
33 incorporates electrode pads 3 on its inner surface and is

1 attached to a process layer 4 that incorporates channel  
2 and cavity structures containing chemical reagents,  
3 together they comprise the microfluidic assembly 5. A  
4 carrier layer 6 supports and protects item 5 and  
5 incorporates pockets 7. Access holes 8 through item 4 and  
6 6 allow external electrical probes to interface with  
7 electrodes 3. The device is generally planar and is  
8 typically processed in a vertical plane such that its  
9 upper edge presents loading ports to the processing  
10 instrument. In this example, the device has on-board  
11 reagents comprising a separation gel 9 which can be pre-  
12 loaded with a suitable stainer, for example ethidium  
13 bromide, and an electrolytic buffer 10 which fills the  
14 top cavity 11 of the microfluidic assembly 5. The  
15 electrodes 3 comprise an anode 12 within the top cavity  
16 11, a compacting electrode 13 which crosses the capillary  
17 channel 14 immediately above the top of the gel surface  
18 15, and a cathode 16 within the lower cavity 17.

19

20 With reference to Figure 18, bio-molecular separation can  
21 be enabled by

- 22 - loading the sample diluted in a low ionic strength  
23 buffer and mixed with glycerol which causes the  
24 loaded sample to sink under gravity to the lower end  
25 of top cavity 11.
- 26 - Application of a low voltage dc potential (for  
27 example 10 volts) between cathode 12 and anode 16  
28 will cause a DNA sample to rapidly migrate to the  
29 top of the gel surface 15; this method being the  
30 already known method of stacking by use of  
31 discontinuous buffers. Sample migration into the gel  
32 with this voltage is strongly retarded (due to the  
33 higher ionic strength of the gel) for a stacking

1 duration which can be in the range of 5 to 30  
2 seconds.

3 - switch the voltage to a much higher level, for  
4 example in the range of 120 to 200 volts, which  
5 drives the stacked sample into the gel for  
6 separation. A separation column of 20mm in length  
7 will allow separation of a DNA sample in the range  
8 25 to 2000 base pairs when using an agarose gel of  
9 0.8% concentration in typically 60 to 75 seconds.

10

11 With reference to Figure 18, an alternative stacking  
12 method is to use the compacting electrode 13 to compact a  
13 DNA sample loaded into top cavity 11 by switching top  
14 electrode 12 negative and the compacting electrode 13  
15 positive, thereby focussing the sample on the compacting  
16 electrode which is preferably gold or platinum or silver  
17 thereby avoiding chemical affinity between the electrode  
18 and the DNA sample. Typically, the voltage used can be  
19 100V for 20 seconds. The compacting electrode can then be  
20 switched off and the positive charge switched to the  
21 lower electrode 16 at the other end of the separation  
22 channel to separate the sample. Typically this can be  
23 150V for 75 seconds.

24

25 Figure 17b shows an enlargement of the pipette insertion  
26 step of figure 17a, showing an overspill 112 and the  
27 configuration of the flaps 114.

28

29 Further features of the microfluidic device are:  
30 the embodiment of fiducial marks which can be applied  
31 simultaneously with the electrodes 12, 13, and 16 by a  
32 process which can conveniently be screen printing, but

1 may also be ink jet, hot foil, flexo print or other  
2 similar printing techniques; and  
3 the embodiment of a side label which can be used as  
4 handling tab during the loading and unloading of the  
5 microfluidic device onto or from the instrument and can  
6 also be used as an identification label that incorporates  
7 useful data such as the device type, use by date, batch  
8 code and that this data can be in the form of a 1D or 2D  
9 bar code.

10

11 It is a function of the analysis instrument to load the  
12 test sample into top cavity 11 using a pipette tip 24  
13 after first using a piercing tool 40 to penetrate pocket  
14 7 and cavity 11.

15

16 The loaded sample can then be stacked into a narrow band  
17 at the top of the gel using techniques for sample  
18 stacking in either electrophoresis or column  
19 chromatography devices. These include, for example, the  
20 use of discontinuous buffers in which the sample is  
21 diluted or the transient application to the sample of  
22 much lower voltages than those used for sample  
23 separation.

24

25 With reference to Figure 18, a further alternative method  
26 of utilising the three electrodes is:

27 apply voltage between electrodes 12 and 16 at low dc  
28 voltage (typically in the range 2V to 10V) for a period  
29 of approximately 20 seconds to stack the test sample 19  
30 on to the top surface of the gel;

31 apply voltage between electrodes 12 and 13 (typically  
32 150V for 20 seconds) which results in absorbance of any  
33 residual test sample 19 in top cavity 11 into

1 theelectrode 13 which specifically is composed of carbon,  
2 therefore having a high absorbance for DNA (and therefore  
3 avoids smearing during the subsequent separation process  
4 from residual DNA in top cavity 11 since this residual  
5 material is absorbed); and apply voltage between  
6 electrodes 12 and 16 (typically 150V for 60 seconds) to  
7 electro-kinetically move and separate the test sample 19  
8 within capillary channel 14.

9

10 Excite the test sample stainer (for example, ethidium  
11 bromide or cybrgreen) with a light source of appropriate  
12 wavelength and capture an image of the capillary channel  
13 showing the resulting fluorescence pattern displayed by  
14 the separated nucleic acid fragments in channel 14.

15

16 With reference to Figure 19, the above operating sequence  
17 combined with the microscale nature of the microfluidic  
18 device combined with the automated handling described in  
19 Figures 3a and 3b will enable one microfluidic device  
20 (which can incorporate up to at least 16 parallel test  
21 segments) to be processed in less than six minutes and in  
22 three steps. This compares favourably with an equivalent  
23 slab gel process which can typically take around 135  
24 minutes involving 22 process steps.

25

26 Advantageously, the present invention provides a highly  
27 compact, automated, simple to use, rapid and efficient  
28 means of providing bio-analysis results, and in  
29 particular, when this involves electro-phoretic  
30 separation.

31

32 Improvements and modifications may be incorporated herein  
33 without deviating from the scope of the invention.

**Claims**

1. An analysis instrument for processing a microfluidic device, comprising sample storage means, a microfluidic device holder, sample loading means for loading sample into a microfluidic device disposed in the holder, processing means for enabling a reaction in a microfluidic device, and detection means for detecting and/or measuring the reaction, characterised in that the microfluidic device holder is adapted to hold the microfluidic device comprising or including a tape in position for processing and/or detection.
2. An instrument according to claim 1, wherein the sample loading means is moveable relative to the sample storage means and relative to the microfluidic device holder.
3. An instrument according to claim 1 or claim 2, further comprising opening means for opening a microfluidic device.
4. An instrument according to claim 3, the sample loading means and the microfluidic device opening means being disposed a fixed distance apart on a moveable common support and spaced such that the sample loading means can acquire sample from the sample storage means whilst at the same time the microfluidic device opening means opens the microfluidic device.
5. An instrument according to claim 3 or claim 4, the sample loading means comprising a nozzle, the nozzle being adapted to removably mount a pipette tip, the nozzle further being operably attached to a pump for pumping liquid into a mounted pipette tip.
6. An instrument according to claim 5, including means for removal of a used pipette tip from the nozzle.

7. An instrument according to claim 6, the removal means comprising a flange, the pipette tip being removed by relative movement between the mounted pipette tip and the flange.
- 5 8. An instrument according to claim 7, including a receptacle for receiving a spent pipette tip.
9. An instrument according to any of claims 5 to 8, including a fresh pipette tip store adapted to store pipette tips such that the nozzle can be  
10 brought into contact with a pipette tip for attachment to the nozzle.
10. An instrument according to claim 9 when dependant upon claim 8, the receptacle and the store being parts of a single demountable unit.
- 15 11. An instrument according to any of claims 4 to 10, wherein the opening means comprises a piercing tool, removably mounted on the moveable common support.
12. An instrument according to claim 11, wherein the piercing tool  
20 comprises a needle.
13. An instrument according to claim 11 or claim 12, including means for removal of a used needle from the moveable common support.
- 25 14. An instrument according to claim 13, the removal means comprising a flange, the used needle being removed by relative movement between the needle and the flange.
- 30 15. An instrument according to claim 14, including a receptacle for receiving a used needle.

16. An instrument according to any of claims 12 to 15, including a fresh needle store adapted to store needles such that the common support can be brought into contact with a needle for attachment thereto.
- 5 17. An instrument according to claim 16 when dependant upon claim 15, the receptacle and the store being parts of a single demountable unit.
18. An instrument according to any of claims 12 to 17, adapted to maintain a count of needle usage to alert a user to a requirement for needle  
10 changeover.
19. An instrument according to any preceeding claim, operable to process a single sample using one single element of a microfluidic device.
- 15 20. An instrument according to claim 19, operable to process a single sample using one single element of a microfluidic device by comprising a single sample loading means only, the single sample loading means being enabled to load sample one sample at a time from a plurality of sample holders, and deliver each said sample to a separate element of a microfluidic  
20 device.
21. An instrument according to any preceeding claim, operable to permit a batch of multiple samples to be processed up to the limit of the test element capacity of a single microfluidic device.  
25
22. An instrument according to any of claims 1 to 18, operable to permit a batch of multiple samples to be processed up to the limit of the capacity of a microfluidic device feeder module.
- 30 23. An instrument according to any preceeding claim, the sample storage means being mounted on a platform, moveable relative to the sample



detection means.

24. An instrument according to any preceding claim, wherein the sample  
detection means and the microfluidic device holder are moveable relative to  
5 one another to allow samples within the microfluidic device to be positioned  
at a predetermined location for detection.

25. An instrument according to any preceding claim, wherein the  
microfluidic device holder is adapted to accommodate a microfluidic device  
10 having a plurality of microfluidic processing elements such that each said  
element can be individually detected by the detection means.

26. An instrument according to any preceding claim, wherein the  
microfluidic device holder is mounted on the same platform as the sample  
15 storage means.

27. An instrument according to any preceding claim, wherein the sample  
processing means comprises a plurality of probes for applying voltage to a  
sample in a microfluidic device mounted in the holder.  
20

28. An instrument according to claim 27, wherein the probes are disposed  
to contact conductive pads of the microfluidic device.

29. An instrument according to claim 27 or claim 28, adapted to enable  
25 electro-phoretic separation of a sample containing, molecules of DNA or  
RNA or proteins.

30. An instrument according to claim 27 or claim 28, adapted to enable  
electro-kinetic transport of a biological sample past a zone within the  
30 microfluidic device that contains one or more antibodies, such that binding  
between the sample and any antibody material can be enabled.

31. An instrument according to any preceding claim, wherein the detection means is adapted to detect change in conductivity in a sample.
- 5 32. An instrument according to any of claims 1 to 30, wherein the sample detection means comprises an optical assembly.
33. An instrument according to claim 32, wherein the optical assembly includes a light source capable of emitting at a predetermined first frequency  
10 for excitation of constituents of the sample to allow the sample to emit light at a second frequency, and a light receiver.
34. An instrument according to claim 33, wherein the receiver comprises a charged coupled device, or a line scan camera.
- 15 35. An instrument according to claim 33 or claim 34, wherein the receiver is configured to send image data to an external data processing device.
36. An instrument according to any preceding claim, including an on-  
20 board system controller, the controller being programmable by a user to perform automated microfluidic device processing.
37. An instrument according to any of claims 1 to 35, adapted to be controlled by an external system controller.
- 25 38. An instrument according to any preceding claim, including a feeder module removeably attachable to the instrument and storing multiple microfluidic devices for automatic loading into or unloading from the microfluidic device holder.
- 30 39. An instrument substantially as hereinbefore described with reference

to the accompanying drawings.

- 5 40. A microfluidic processing device, comprising a reaction chamber, a sample loading chamber into which a sample is injectable, the reaction chamber being operatively connected to the sample loading chamber, a cover that extends across at least part of the sample loading chamber, the cover and the reaction chamber comprising pierceable material and being separated by an overspill cavity configured to accept any overspill of an injected sample.
- 10 41. A microfluidic processing device according to claim 40, wherein the reaction chamber contains a molecular separation medium.
42. A microfluidic processing device according to claim 40 or claim 41, wherein the reaction chamber is a channel.
- 15 43. A microfluidic processing device according to claim 42, wherein the microfluidic processing device further includes a receiving chamber at an end of the reaction channel remote from the sample loading chamber.
- 20 44. A microfluidic processing device according to any of claims 41 to 43, wherein the cover and/or the loading chamber are manufactured from polymer film.
- 25 45. A microfluidic processing device according to any of claims 40 to 44, having a laminated structure.
- 30 46. A microfluidic processing device according to any of claims 40 to 45, including optical fiducial marks whose position is known relative to the reaction chamber and which can be acquired by the detection means of an analysis instrument to accurately identify the position of a reaction process.

47. A microfluidic processing device substantially as hereinbefore described with reference to the accompanying drawings.

5 48. A kit comprising an analysis instrument according to any of claims 1 to 39 and a microfluidic processing device according to any of claims 40 to 45.



For Innovation

45

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**Examiner:** Mr Stuart Purdy

**Claims searched:** 1-39 & 48

**Date of search:** 5 June 2006

## Patents Act 1977: Search Report under Section 17

### Documents considered to be relevant:

Category	Relevant to claims	Identity of document and passage or figure of particular relevance
X	1-3, 5-9, 11, 12, 19-30, 32-38 at least	WO 2005/114223 A1 (CALIPER LIFE SCIENCES) see whole document and in particular p. 3 ln 26-30, p6 ln 25-32, p7 ln 1-4, ln10-14, 19-21, 34- p8 ln 5, p8 ln 13-15, p11 ln 9-10, p12 ln 16-18, & p14 ln 23-30;
X	1, 2, 19-26, 32-38	EP 1403644 A1 (AGILENT TECHNOLOGIES) see whole document and in particular para 1, 22, 26-28, 31-34;
X	1, 2, 19-25, 27-29, 32-37 at least	US 2005/0220675 A1 (REED) see whole document and in particular note paras 199, 299, 532;

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Worldwide search of patent documents classified in the following areas of the IPC

B01F; B01L; B81B; F15C; G01N
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The following online and other databases have been used in the preparation of this search report

WPI & EPODOC
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