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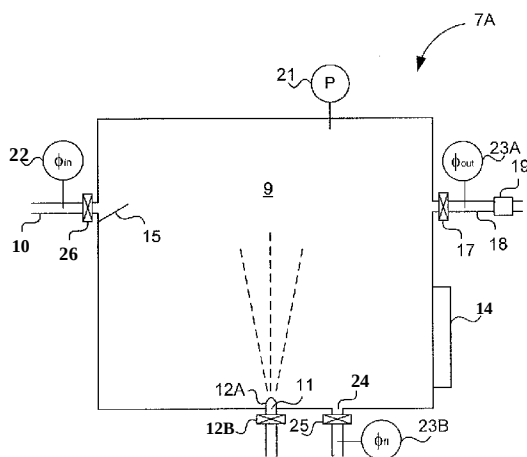


FIG 2

(57) Abstract: The invention relates to a new type of vaporiser arrangement (7) for a breathing apparatus (1), serving the double purpose of vaporiser and pressurised supply of vapour-containing gas for direct delivery to a patient (2). The vaporiser arrangement (7) comprises at least a first gas inlet channel (10) for conveying a flow of a carrier gas into a vaporisation chamber (9), vaporisation means (12) for vaporising a liquid into the carrier gas in the vaporisation chamber, and a gas outlet channel (18) for conveying a flow of vapour-containing carrier gas out of the vaporisation chamber and towards the patient (2). The vaporiser arrangement (7) further comprises gas flow regulating means (17, 25, 26) configured to maintain the carrier gas within the vaporisation chamber (9) at an overpressure, and to control the flow of vapour-containing carrier gas out of the vaporisation chamber in a variable manner.

VAPORISER ARRANGEMENT FOR BREATHING APPARATUS

TECHNICAL FIELD

The present invention relates to a vaporiser arrangement for a breathing
5 apparatus according to the preamble of claim 1, and a breathing apparatus
according to the preamble of claim 17. It also relates to a gas tank
arrangement according to the preamble of claim 21, and a gas tank
arrangement according to the preamble of claim 31.

10 BACKGROUND ART

In breathing apparatuses vaporised liquid, such as vaporised anaesthetic or
vaporised water, is often added to the breathing gas before the breathing gas
is delivered to the patient. Normally, a flow of gas is directed through a
vaporisation chamber in which it absorbs the vaporised liquid before being
15 delivered to the patient, either directly or after subsequent mixing with
additional gas components.

For example, in certain types of anaesthesia apparatuses, a flow of fresh gas
is directed through a vaporisation chamber of an anaesthetic vaporiser, in
which it absorbs vaporised anaesthetic liquid. Examples of anaesthetic
20 vaporisers are disclosed in e.g. EP 0958842 and EP1 402961. These
documents disclose injection vaporisers wherein fine droplets of volatile
anaesthetic liquid is injected into a flow of breathing gas passing through the
vaporisation chamber. Another type of anaesthetic vaporiser is the so called
flow-by vaporiser wherein the flow of breathing gas simply passes over a
25 surface of liquid anaesthetic within the vaporisation chamber.

This flow-by principle is often used also in water vaporisers, often referred to
as humidifiers. Humidifiers are often used in ventilators in order to humidify
breathing gas before the breathing gas is delivered to the patient undergoing

the ventilatory treatment. Humidifying the breathing gas is desirable since the gas delivered by the ventilator is dry, which may cause the patient to be dried out and cooled down. In flow-by humidifiers, a flow of gas is conveyed through a vaporisation chamber in which it passes over or through heated water in order to absorb water vapour before being delivered to the patient. Normally, in both anaesthesia apparatuses and ventilators, the gas that is directed through the vaporiser chamber in order to absorb the vaporised liquid, hereinafter referred to as the carrier gas, passes freely through the vaporisation chamber and onto the patient or a subsequent mixing stage where the vapour-containing gas is mixed with other gas components before delivery to the patient.

One problem associated with this "free flow technique" is that the carrier gas is unable to absorb a sufficient amount of vaporised liquid on its way through the vaporisation chamber and hence that the humidity of the breathing gas, or the concentration of anaesthetic agent in the breathing gas, is too low when delivered to the patient. This is particularly relevant for high flows of carrier gas.

Another problem is that the concentration of vapour-content in the gas flow from the vaporiser varies substantially if the gas flow through the vaporiser varies. This is because low flows give the gas more time to absorb the vapour within the chamber than high flows, and also because high flows decreases the rate of vaporisation in the vaporisation chamber as they cool down the often heated vaporisation chamber. This fact makes it hard to deliver varying flows of vapour-containing gas with constant vapour-content to the patient.

In some applications where low flows of carrier gas are used, the problem is the opposite, namely that the vapour concentration becomes too high if the entire flow of carrier gas is directed through the vaporisation chamber. Therefore, there are vaporisers according to prior art wherein the flow of carrier gas is divided into two separate flows upstream of the vaporisation

chamber; one which is directed through the vaporisation and one that bypasses the vaporisation chamber. The two separate flows are then mixed again, downstream of the vaporisation chamber. Here too, it is very hard to maintain a stable vapour concentration in the carrier gas, especially if the
5 flow of carrier gas through the vaporisation chamber varies over time.

Yet another problem which mainly relates to flow-by vaporisers (and not injection vaporisers) is that the vapour content in the relatively small vaporisation chamber is quickly absorbed by the flow of carrier gas, which also makes the vapour concentration in the vapour-containing gas vary in
10 time. This effect is further enhanced by the fact that the flow of carrier gas passing over or through the liquid in the vaporisation chamber cools the liquid, which reduces the rate of vaporisation.

A slightly different problem related to breathing apparatuses equipped with vaporiser arrangements is the complexity of the gas flow circuit. In both
15 anaesthesia apparatuses and ventilators there is often a desire to use a carrier gas in form of a well-defined gas mixture comprising two or more gas components, such as a mixture of air, oxygen, and/or nitrous oxide.

Therefore, the carrier gas is often a gas mixture formed in a gas mixing chamber disposed upstream of the vaporisation chamber and connected in
20 series therewith. An example of a gas mixing chamber suitable for this purpose is the receiver tank 12 of Fig. 1 in US 5 383 449. There is a desire to reduce the complexity and hence the cost of this type of gas flow circuits where there is a need for vaporisation of liquid into a multi-component gas mixture.

25

SUMMARY OF THE INVENTION

It is an object of the present invention to provide a vaporiser arrangement that solves or at least mitigates one or more of the above mentioned
30 problems. In particular, it is an object of the invention to provide a vaporiser

arrangement that is capable of delivering varying flows of vapour-containing gas with a substantially stable vapour concentration.

This object is achieved by a vaporiser arrangement for a breathing apparatus, comprising:

- 5 - at least a first gas inlet channel for conveying a flow of a carrier gas into a vaporisation chamber;
 - vaporisation means for vaporising a liquid into the carrier gas in the vaporisation chamber, and
 - a gas outlet channel for conveying a flow of vapour-containing carrier gas
- 10 out of the vaporisation chamber and towards a patient.

The vaporiser arrangement further comprises gas flow regulating means operable to maintain the carrier gas within the vaporisation chamber at an overpressure, and to control the flow of vapour-containing carrier gas out of the vaporisation chamber in a variable manner.

- 15 To this end, the gas flow regulating means may comprise a controllable valve arranged in the gas outlet channel.

- That the gas flow regulating means is capable of maintaining the carrier gas in the vaporisation chamber means that the gas flow regulating means is configured to temporally interrupt the flow of vapour-containing carrier gas
- 20 out of the vaporisation chamber or at least temporally make the flow of vapour-containing carrier gas out of the vaporisation chamber less than the flow of carrier gas into the vaporisation chamber.

- An effect of maintaining the carrier gas in the vaporisation chamber is that the concentration of the vaporised liquid in the carrier gas can be increased
- 25 compared to prior art solutions in which the carrier gas passes freely through the vaporisation chamber. This is because the carrier gas has more time to absorb the vaporised liquid. This is particularly useful in high-flow applications where high flows of vapour-containing gas are to be delivered to the patient.

That the carrier gas is maintained in the vaporisation chamber further has the effect of mitigating undesired variations in concentration of the vapour component in the vapour-containing carrier gas leaving the vaporisation chamber. This is because the carrier gas/vapour mixture will have more time
5 to form a homogeneous gas mixture within the vaporisation chamber.

That the carrier gas is maintained at an overpressure means that the pressure in the vaporisation chamber is higher than the pressure in the gas outlet channel.

The effect of maintaining the carrier gas at an overpressure is that the carrier
10 gas that is maintained in the vaporisation chamber can be delivered to the patient under influence of the elevated pressure in the vaporisation chamber. This means that no external flow generating means has to be used to supply the vapour-containing carrier gas from the vaporisation chamber to the patient. Another effect is that the vaporisation chamber is capable of storing a
15 larger volume of vapour-containing gas at the elevated pressure, for subsequent delivery to the patient.

Maintaining the carrier gas at an overpressure in the vaporisation chamber further has the effect that a large volume of vapour-containing gas can be "prefabricated" for subsequent delivery to the patient. This is particularly
20 useful in low flow applications where low flows of vapour-containing gas are to be delivered to the patient. For example, in ventilation of neonatal patients having a tidal volume of just a few millilitres it is difficult to deliver a low flow of vapour-containing carrier gas having a substantially constant vapour-component concentration using free-flow vaporisers according to prior art.
25 Especially when using injection vaporisers having a certain minimum injection volume of liquid. In free-flow vaporisers according to prior art it may also be difficult to monitor the vapour-component concentration in low flows of vapour-containing gas since the amount of the vapour-component in the small volume of gas available for measurement put high demands on the
30 sensitivity of the gas analysers and introduces a high degree of uncertainty in

- gas composition measurements. By maintaining a large volume of carrier gas (several times the tidal volume of neonatal patients) in the vaporisation chamber, a low flow of prefabricated and homogeneously mixed vapour-containing gas can be delivered from the vaporisation chamber under the
- 5 control of the gas flow regulating means. Furthermore, gas composition determination can be carried out on the large volume of gas in the vaporisation chamber, which increases the accuracy in the determination of the vapour-component concentration in the gas that is to be delivered to the patient.
- 10 Thus, at least to some extent, the proposed vaporiser arrangement forms a new type of vaporiser arrangement having a combined vaporisation chamber and pressurised storage tank for vapour-containing gas.

- Due to the above mentioned advantages following the maintenance of the carrier gas in the vaporisation chamber at an overpressure, the vaporiser
- 15 arrangement is capable of delivering a varying flow of gas having a much more stable concentration of the vapour component than vaporiser arrangements according to prior art.

- The capability of delivering a varying flow of vapour-containing gas with a stable vapour concentration is advantageous in that said flow can be varied
- 20 based on patient-related and/or application-related parameters while still delivering a well-defined dose of the vapour-component to the patient. For example, the flow regulating means may be configured to vary the flow of vapour-containing gas out of the vaporisation chamber based on any of, or any combination of:

- 25 - pressure and/or flow measurements obtained downstream of the vaporisation chamber,
- gas composition measurements obtained in and/or downstream of the vaporisation chamber,
 - a preset tidal volume,

- a preset patient pressure, and
- a preset fresh gas flow.

Preferably, the flow regulating means is operable to control also the flow of carrier gas into the vaporisation chamber. To this end, the gas flow regulating means may comprise a controllable valve arranged in the gas inlet channel. Active control of the flow of carrier gas into the vaporisation chamber is not a necessity if the carrier gas is delivered to the gas inlet channel at a suitable overpressure. However, it is advantageous since vapour-containing carrier gas otherwise might have to be released through a flush valve or the like in order to avoid pressure build-up in the vaporisation chamber, which pressure build-up otherwise would cause too high flows of vapour-containing gas to the patient.

The flow of carrier gas into the vaporisation chamber is preferably controlled based on measurements indicative of the pressure within the vaporisation chamber. Such measurements may be obtained by measuring the pressure within the vaporisation chamber, or by measuring the flows into and out of the vaporisation chamber. In some applications it may also be advantageous to control the flow of carrier gas into the vaporisation chamber based on the temperature within the vaporisation chamber and/or the gas composition in or downstream of the vaporisation chamber.

Thus, according to a preferred embodiment of the invention, the flow regulating means is operable to control both the flow of carrier gas into the vaporisation chamber and the flow of vapour-containing carrier gas out of the vaporisation chamber. Preferably, the outflow of vapour-containing gas is controlled based on the pressure and/or flow measurements obtained downstream the vaporisation chamber, indicative of the respiratory phase of the patient, and the inflow of carrier gas is controlled based on a parameter that is indicative of the pressure within the vaporisation chamber. This allows the flow of vapour-containing carrier gas from the vaporisation chamber to be synchronised with the respiratory phases of the patient.

Preferably, the flow regulating means is configured to control said inflow and outflow such that during expiration of the patient, the outflow is either interrupted or decreased to a low bias flow, while the inflow is controlled such that a desired overpressure is obtained in the vaporisation chamber. When
5 the desired overpressure is obtained, the inflow of carrier gas is preferably interrupted. During inspiration of the patient, the outflow is increased and controlled such that a desired flow of vapour-containing carrier gas is delivered to the patient, whereby the pressure in the vaporisation chamber decreases and the procedure starts over again. During inspiration of the
10 patient, the flow of carrier gas into the vaporisation chamber may be controlled to prevent the pressure in the vaporisation chamber to fall too much. In other embodiments, however, flow of carrier gas into the vaporisation chamber may be prevented during inspiration of the patient.

In some embodiments, the gas flow regulating means may be operable to
15 fully interrupt the flow of vapour-containing gas out of the vaporisation chamber, at least during expiration phases of the patient. This type of "semi-closed vaporiser arrangement" is advantageous in that it can be ascertained that the carrier gas is maintained in the vaporisation chamber at least for a minimum period of time before being delivered to the patient during
20 inspiration. It is also advantageous in that it provides for fast pressure build-up within the vaporisation chamber during interruption of the outflow, thereby allowing higher flows of vapour-containing gas to be delivered to the patient after the interruption. Another advantage with the semi-closed vaporiser arrangement is that the flow of vapour-containing gas from the vaporisation
25 chamber can be stopped if it is found that too high doses of the vapour-component is or has been delivered to the patient. Therefore, the gas flow regulating means is preferably also capable of interrupting the flow of vapour-containing gas out of the vaporisation chamber during inspiration phases of the patient.

Preferably, the gas flow regulating means is configured to maintain the carrier gas in the vaporisation chamber at an overpressure that never exceeds a maximum pressure threshold value.

That the overpressure never exceeds a maximum threshold value has the effect of avoiding too high flows of vapour-containing gas to the patient should the flow regulating means malfunction, e.g. should an outlet valve in the gas outlet channel get stuck in a fully open position. This is particularly important in ventilation of patients with reduced lung capacity (e.g. small patients) where high flows of breathing gas could damage the pulmonary system of the patient.

The gas flow regulating means is preferably configured to control the flow of gas into and out of the vaporisation chamber such that the maximum pressure threshold value is obtained at the end of expiration of the patient (i.e. just before transition from an expiratory phase to an inspiratory phase of the patient). The maximum pressure threshold value can hence be seen as a target pressure for the pressure in the vaporisation chamber at the end of expiration of the patient, i.e. as an end-expiratory target pressure.

Furthermore, the gas flow regulating means is preferably configured to maintain the gas in the vaporisation chamber at an overpressure that always exceeds a certain minimum pressure threshold value. Typically, the pressure in the vaporisation chamber reaches a minimum value at the end of inspiration of the patient (i.e. just before transition from an inspiratory phase to an expiratory phase). The pressure in the vaporisation chamber at the end of an inspiration phase of the patient will hereinafter be referred to as the end-inspiratory pressure in the vaporisation chamber. The gas flow regulating means may hence be configured to keep this end-inspiratory pressure above a minimum inspiratory pressure threshold value.

The effect of always maintaining the pressure in the vaporisation chamber above a certain minimum value has the effect of always being able to deliver

a certain minimum flow to the patient. This is important in order to deliver a sufficient dose of the vapour-component to the patient, and, in applications where the vaporiser arrangement is used to deliver the entire tidal volume to an adult patient with high lung capacity, to be capable of delivering the entire tidal volume during the time of an inspiration phase. The ability to deliver a certain minimum flow may also be important in situations where the patient flow must be maintained above a certain threshold value in order to keep the airways of the patient open.

In some embodiments, flow of carrier gas into the vaporisation chamber is prevented during inspiration phases of the patient, and the end-expiratory target pressure is set high enough to ensure that the pressure in the vaporisation chamber does not fall below the minimum pressure threshold value during the end of the inspiration phases.

In other embodiments, the end-expiratory target pressure may not be that high and flow of carrier gas into the vaporisation chamber during inspiration phases may be permitted and controlled by the gas flow regulating means such that the pressure in the vaporisation chamber is maintained above the minimum pressure threshold value throughout the entire inspiration phases.

Thus, the gas flow regulating means of the vaporiser arrangement according to the invention is preferably configured to control the flow of carrier gas into the vaporisation chamber and the flow of vapour-containing carrier gas out of the vaporisation chamber such that the overpressure in the vaporisation chamber is always maintained between a minimum pressure threshold value and a maximum pressure threshold value.

These maximum and minimum pressure threshold values are preferably selected based on one or more design parameters, including but not limited to the tidal volume of the currently ventilated patient, the dynamics of an outlet valve arranged in the gas outlet channel for controlling the flow of vapour-containing carrier gas out of the vaporisation chamber, and a desired

minimum and/or maximum flow of vapour-containing gas out of the vaporisation chamber.

Not only the overpressure at which the carrier gas is maintained in the vaporisation chamber but also the volume of the vaporisation chamber is a design parameter that should be adapted to the intended use of the vaporiser arrangement, and so to the above listed parameters. Yet another parameter that must be taken into account when it comes to the volume of the vaporisation chamber is design requirements regarding the size of the vaporiser arrangement.

- 10 Preferably, the volume of the vaporisation chamber should be between 500 ml and 4000 ml where the larger chamber is optimized for situations in which the carrier gas is delivered to the vaporisation chamber at a pressure of approximately 0,5 bar and the smaller chamber is optimized for situations in which the carrier gas is delivered at a pressure approximately 4 bar. With an outlet valve being able to deliver a desired flow to the patient, preferably
15 above 120 lpm within the pressure range of the chamber (i.e. between the minimum and maximum pressure threshold values), the chamber will be able to deliver a tidal volume of 1000 ml with no restrictions apart from the maximum flow limit set by the valve.
- 20 Typical gas flow valves suitable for use in this type of applications have operational ranges making them capable of maintaining a flow through the valve above a given threshold value as long as the pressure drop over the valve is no more than half the starting pressure. Therefore, the minimum pressure threshold value is preferably half the maximum pressure threshold
25 value or more, and the outlet valve is preferably adapted to permit flows above 120 lpm within this pressure range. Furthermore, the volume of the vaporisation chamber is preferably selected such that said desired flow (e.g. at least 120 lpm) can be delivered during a time period making the delivered volume of vapour-containing gas correspond to at least a tidal volume of an
30 adult patient with normal lung capacity, i.e. a volume of at least 600 ml.

Even more preferably, the volume of the vaporisation chamber is selected such that some gas will remain in the vaporisation chamber even if the entire tidal volume of gas is delivered to an adult patient with normal lung capacity from the vaporisation chamber during an inspiration phase. This has the effect that at least some carrier gas may be maintained in the vaporisation chamber during at least one respiratory cycle (i.e. an inspiration phase and an expiration phase), thus providing for even higher and even more stable concentrations of vapour in the vapour-containing carrier gas delivered to the patient.

10 In a preferred embodiment of the invention making the vaporiser arrangement suitable for most situations, the volume of the vaporisation chamber is at least 2000 ml and the flow regulating means is operable to obtain an end-expiratory pressure in the vaporisation chamber of at least 1 bar, relative to the pressure in the gas outlet channel. A vaporisation
15 chamber volume of at least 2000 ml and a relative end-expiratory pressure of at least 1 bar ensure that the vaporiser arrangement is capable of delivering a flow of vapour-containing carrier gas of at least 120 l/min at half the end-expiratory pressure, i.e. at a relative pressure of 0,5 bar. This means that the vaporiser arrangement will be capable of delivering a volume of at least 1 litre
20 of vapour-containing carrier gas to the patient, even during short inspiratory phases, with a flow that never falls below 120 l/min. In embodiments where the gas flow regulating means comprises a controllable outlet valve for controlling the flow of vapour-containing gas out of the vaporisation chamber, the dynamics of the outlet valve should be adapted to allow flows of at
25 least 120 lpm through the valve at an overpressure of 0,5 bar upstream the valve.

In another exemplary embodiment of the invention, the vaporisation chamber has a volume of approximately 1000 ml, the end-expiratory target pressure in the vaporisation chamber is approximately 2 bar, and the minimum pressure
30 threshold value in the vaporisation chamber is approximately 1 bar.

In yet another exemplary embodiment of the invention, the vaporisation chamber has a volume of approximately 500 ml, the end-expiratory target pressure in the vaporisation chamber is approximately 4 bar, and the minimum pressure threshold value in the vaporisation chamber is
5 approximately 2 bar.

Thus, in order to deliver sufficiently large tidal volumes of vapour-containing gas at sufficiently high flows, even at relatively low inlet pressures (i.e. when the carrier gas is delivered at relatively low pressures to the vaporisation chamber), the volume of the vaporisation chamber should be at least 500 ml,
10 preferably at least 1000 ml, and even more preferably at least 2000 ml.

In all exemplary embodiments, the outlet valve of the vaporiser arrangement is preferably adapted to deliver a flow of at least 120 lpm within the pressure range defined by the end-expiratory target pressure (i.e. the maximum pressure threshold value) and the minimum pressure threshold value. It
15 should be appreciated that all vaporisation chamber pressures discussed above are pressures relative to the pressure in the gas outlet channel of the vaporiser arrangement. In embodiments where the gas flow regulating means comprises a controllable outlet valve to control the flow of vapour-containing gas out of the vaporisation chamber, this corresponds to the
20 pressure upstream the outlet valve relative to the pressure downstream the outlet valve. Normally, the absolute pressure in the gas flow circuit of a breathing apparatus (including the gas outlet channel) is approximately 1 atmosphere, or a few cmH₂O above 1 atmosphere.

In cases where the vaporiser arrangement is used to deliver very small tidal
25 volumes to the patient, it should be appreciated that the end-expiratory target pressure may be reduced substantially. If, for example, the maximum tidal volume of the patient is no more than 50 ml, the gas flow regulating means may be configured to maintain the carrier gas in the vaporisation chamber at an overpressure that never exceeds 0,025 bar relative to the pressure in the
30 gas outlet channel.

In some embodiments, a compressor may be used to deliver pressurised carrier gas to vaporisation chamber. Such a compressor may be included in the vaporiser arrangement or the breathing apparatus of which the vaporiser arrangement forms a part. The compressor for the vaporisation chamber
5 shall be designed to deliver the minute volume desired by the breathing apparatus, and preferably more than 30 lpm. The above described preferred embodiment of the invention ensures that the vaporiser arrangement can be used to deliver the entire tidal volume of gas to the patient when used together with such a compressor, even when large tidal volumes have to be
10 delivered to the patient at high flows.

In other embodiments, the carrier gas may be supplied to the vaporisation chamber directly from a wall outlet delivering carrier gas at a pressure of approximately 4 bar. In embodiments where the gas inlet channel(s) of the vaporiser arrangement is connected directly to such a wall outlet, the end-
15 expiratory target pressure in the vaporisation chamber maybe set to approximately 4 bar, while the minimum pressure threshold value may be approximately 2 bar. In this case a vaporisation chamber volume of 0,5 litre is sufficient in order to deliver more than one litre of vapour-containing gas to the patient with a flow that never falls below 120 lpm. It should further be
20 noted that if the outflow from the vaporisation chamber is controlled by means of a controllable outlet valve, the dynamics of said outlet valve also has impact on the vaporiser arrangement's capability of delivering high flows. To this end, the gas flow regulating means may be configured to control the overpressure in the vaporisation chamber based on the dynamics of such an
25 outlet valve.

As indicated above, the vaporiser arrangement may be adapted to deliver an entire tidal volume of vapour-containing gas to the patient. This opens up for new uses of the vaporiser arrangement. For example, as will be described below with reference to Figs. 1 and 2, the vaporiser arrangement may be
30 used in an anaesthesia apparatus to deliver a flow of fresh gas that is

subsequently added to an inspiration branch of a circle system in which exhalation gases exhaled by the patient are resupplied to the patient after removal of carbon dioxide. The capability of the vaporiser arrangement to deliver an entire tidal volume to the patient and to synchronise the delivery of gas with the respiratory phases of the patient makes it possible to disconnect the circle system and to ventilate the patient only by means of the vaporiser arrangement.

The vaporiser arrangement is particularly intended to serve as an anaesthetic vaporiser for vaporisation of anaesthetic liquid or as a humidifier for vaporisation of water. However, the vaporiser arrangement may also be used for vaporisation of other liquids, such as other medical liquids having a therapeutic effect on a patient being connected to the breathing apparatus. It is also contemplated that the vaporiser arrangement may be used for simultaneous vaporisation of more than one type of liquid into the carrier gas.

According to another aspect of the invention, the vaporiser arrangement comprises a first gas inlet channel and at least a second gas inlet channel for introducing a first and a second gas, respectively, into the vaporisation chamber, so as to allow the first gas and second gas to mix within the vaporisation chamber to form said carrier gas. The gas flow regulating means of the vaporiser arrangement may then be operable to control the flows of the first and second gas through the first and second gas inlet channels in dependence of each other so as to obtain a desired gas mixture as said carrier gas.

Thus, according to this aspect of the invention, not only does the vaporiser arrangement serve as a combined vaporiser and storage tank, it also serves as a gas mixing chamber. By letting the mixing of gas components forming the carrier gas, and the vaporisation of liquid into the carrier gas, take place within the same space, i.e. within the vaporisation chamber, the number of components in the gas flow circuit, and hence the complexity and cost of the gas flow circuit, can be reduced.

To allow mixing of more gas components, the vaporisation chamber may comprise yet further gas inlets. For example, the vaporisation chamber may comprise three gas inlets for introduction of air, oxygen and nitrous oxide, respectively, into the vaporisation chamber.

- 5 In embodiments where the vaporiser arrangement comprises a plurality of gas inlet channels for a respective carrier gas component, the flow of the respective carrier gas component into the vaporisation chamber is preferably, in addition to the pressure in the vaporisation chamber, controlled based on gas composition measurements and/or settings, so as to obtain a desired
- 10 carrier gas mixture within the vaporisation chamber and hence a desired gas mixture for delivery to the patient. The gas composition measurements can be obtained by means of a gas analyser arranged within the vaporisation chamber or the gas outlet channel, and/or by a gas analyser arranged in closer proximity to the patient, for example in a Y-piece of the breathing
- 15 apparatus.

Preferably, where the vaporiser arrangement comprises a plurality of gas inlet channels, the flow regulating means comprises a controllable valve in each of the respective gas inlet channels.

- To achieve efficient mixing of any carrier gas components and the vapour
- 20 component within the vaporisation chamber, the gas inlet channel(s) and the gas outlet channel may be arranged in relation to each other so as to create a high degree of turbulence within the vaporisation chamber. Instead or in addition to a certain arrangement of the gas inlet and outlet channels, the vaporiser arrangement may comprise turbulence generating means arranged
- 25 to further increase the turbulence within the vaporisation chamber. The turbulence generating means may comprise a fan for generating a forced flow within the vaporisation chamber, and/or flow benders for redirecting the natural flow of carrier gas or carrier gas components entering the vaporisation chamber through the gas inlet channel(s).

The vaporiser arrangement may be designed as an injection vaporiser. In this case, the vaporisation means for vaporisation of the liquid into the carrier gas may comprise an injection nozzle for injecting fine droplets of liquid into the carrier gas in the vaporisation chamber and a liquid flow control valve for
5 controlling the flow of liquid through the injection nozzle.

The vaporiser arrangement may also be designed as a flow-by vaporiser. In this case, the vaporisation means may comprise nothing but a receptacle for holding a volume of liquid to be vaporised into the carrier gas. The receptacle may be a lower portion of the vaporisation chamber.

10 The present invention also concerns a breathing apparatus comprising a vaporiser arrangement as described above. The breathing apparatus may be an anaesthesia apparatus wherein the vaporiser arrangement is an anaesthetic vaporiser for adding anaesthetic agent to a breathing gas. The breathing apparatus may also be a conventional ventilator or any other
15 device for providing respiratory support to a patient, wherein the vaporiser arrangement is a humidifier for humidifying a breathing gas through vaporisation of water.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 illustrates an embodiment of a breathing apparatus according to the
20 invention.

Fig. 2 illustrates an embodiment of a vaporiser arrangement according to the invention.

Figs. 3 and 4 illustrate other embodiments of a breathing apparatus according to the invention.

25 Figs. 5 and 6 illustrate other embodiments of a vaporiser arrangement according to the invention.

Fig. 7 illustrates an embodiment of a gas tank arrangement according to one aspect of the invention.

Figs. 8 and 9 illustrate embodiments of a gas tank arrangement according to another aspect of the invention.

5

DETAILED DESCRIPTION

Vaporiser Arrangement for Breathing Apparatus

Fig. 1 illustrates an example of a breathing apparatus 1A according to one
10 embodiment of the invention.

In this embodiment, the breathing apparatus 1A is an anaesthesia apparatus for delivery of inhalation anaesthetic to a patient 2 during respiratory treatment. The anaesthesia apparatus comprises a drive unit 3, which may comprise a ventilator, for the supply and regulation of breathing gases. It
15 further comprises a breathing circuit which, in this embodiment, is a circle system comprising an inspiratory branch 4 and an expiratory branch 5. Gases exhaled by the patient 2 are conveyed through the expiratory branch 5 and resupplied to the patient 2 via the inspiratory branch 4 after removal of carbon dioxide by means of a carbon dioxide absorber 6 in the inspiratory
20 branch. Furthermore, the apparatus 1 comprises a vaporiser arrangement 7A for supply of an anaesthetic agent to the patient 2 via a fresh gas supply line 8.

Fig. 2 illustrates the vaporiser arrangement 7A of Fig. 1 in greater detail. With reference simultaneously made to Fig. 1, the vaporiser arrangement 7A is
25 seen to comprise a vaporisation chamber 9 in which liquid anaesthetic is vaporised into a carrier gas for subsequent delivery to the patient 2 via the fresh gas supply line 8. The carrier gas is supplied to the vaporisation chamber 9 via a gas inlet channel 10. The carrier gas may be constituted by a single gas component but is typically a mixture of a plurality of carrier gas

components, such as air, oxygen and nitrous oxide. The carrier gas is delivered to the vaporiser arrangement 7A from the drive unit 3 at an overpressure. To this end, the drive unit 3 may be connected to one or more medical gas wall outlets delivering pressurised medical gases or it may
5 comprise one or more compressors for pressuring the carrier gas. In other embodiments, the vaporiser arrangement itself 7A may comprise means for pressurising the carrier gas, such as one or more compressors.

The vaporiser arrangement 7A is further seen to comprise a liquid inlet 11 for introducing liquid anaesthetic into the vaporisation chamber 9. In this
10 embodiment, the vaporiser arrangement is an injection vaporiser comprising liquid injection means for actively injecting the anaesthetic liquid into the carrier gas. The liquid injection means comprises an injection nozzle 12A and a liquid flow control valve 12B for controlling the flow of liquid anaesthetic through the nozzle 12A and into the vaporisation chamber 9.

15 The vaporiser arrangement 7A may further comprise heating means 14 for heating the vaporisation chamber 9 to a temperature at which a desired degree of vaporisation of the liquid is achieved.

To achieve efficient mixing of the carrier gas components and the vapour component within the vaporisation chamber 9, the vaporiser arrangement
20 may comprise turbulence generating means 15 for increasing the turbulence within the vaporisation chamber. Here, the turbulence generating means 15 are gas flow benders in form of elements protruding from the inner wall of the vaporisation chamber 9 and at least partly into the flow paths of the carrier gas delivered through the gas inlet channel 10. A net arranged near the
25 opening of the gas inlet channel 10 in the vaporisation chamber 9 may also be used as turbulence generating means. Other types of turbulence generating means, such as one or more fans for generating a forced flow of gas in the vaporisation chamber 9, may also be used to increase the turbulence. The turbulence generating means 15 serves to obtain a more

homogeneous mixture of the carrier gas and the vapour component in the vaporisation chamber.

Furthermore, the vaporiser arrangement 7A comprises a gas outlet channel 18 for delivery of the vapour-containing gas from the vaporisation chamber 8 to the patient 2, i.e. for delivery of the carrier gas after absorption of vaporised liquid. In this embodiment, the gas outlet channel 18 is connected to the fresh gas delivery line 8.

The vaporiser arrangement may further comprise a gas analyser 19 for determination of the gas composition of the vapour-containing gas. The gas analyser may be configured to determine the concentration of the vapour component in the carrier gas, but also the concentrations of various gas components in the carrier gas. In this embodiment, the gas analyser 19 is arranged in the gas outlet channel 18. However, the gas analyser may also be arranged within the vaporisation chamber 9.

The vaporiser arrangement comprises gas flow regulating means for maintaining the carrier gas within the vaporisation chamber 8 at an overpressure, and to control the flow of vapour-containing gas out of the vaporisation chamber in a variable manner. This means that the gas flow regulating means is configured to vary said flow based on measured parameters and/or parameter settings set by an operator of the breathing apparatus 1A.

To this end, the gas flow regulating means may comprise a controllable outlet valve 17 which is regulated by a control unit (not shown) of the vaporiser arrangement 7A or the breathing apparatus 1A based on measured parameters, and typically also based on preset parameters set by an operator of the breathing apparatus 1.

The vaporiser arrangement 7A further comprises pressure monitoring means for monitoring the pressure in the vaporisation chamber 9. The pressure monitoring means may comprise a pressure sensor 21 arranged to measure

the pressure in the vaporisation chamber 9, and/or flow sensors 22, 23A-B arranged to measure the flows in and out of the vaporisation chamber, which flows are indicative of the pressure within the vaporisation chamber 9. The pressure monitoring means are coupled to the control unit to allow the gas
5 flow regulating means to be controlled based on the measured pressure and/or flows.

Furthermore, the vaporisation chamber is seen to comprise a flush outlet 24 for flushing gas and/or liquid out of said vaporisation chamber 9. The gas flow regulating means of the vaporiser arrangement is configured to control
10 the flow of gas out of the vaporisation chamber through said flush outlet 24. To this end, the gas flow regulating means may comprise a flush valve 25, also controlled by the control unit of the vaporiser arrangement or the breathing apparatus based on measured and/or preset parameters.

In a basic embodiment of the invention, a flow of pressurised gas is received
15 through the gas inlet channel 10 from one or more gas sources (not shown). The controllable outlet valve 17 is configured to maintain the gas within the vaporisation chamber at an overpressure, relative to the pressure in the gas outlet channel 18, and to control the flow through the gas outlet channel 18 in a variable manner. To avoid too high pressure build-up in the vaporisation
20 chamber 9, the flush valve 25 may be configured to flush excess gas out of the vaporisation chamber 9 when the pressure therein exceeds a maximum threshold value.

In the above described embodiment, it is not required to control the flow of carrier gas into the vaporisation chamber 9 through the gas inlet channel 10.

25 In a preferred embodiment of the invention, however, the gas flow regulating means of the vaporiser arrangement 7A further comprises a controllable inlet valve 26 which is also controlled by the control unit of the vaporiser arrangement or the breathing apparatus 1A based on measured and/or preset parameters.

The outlet valve 17 and the inlet valve 26 may be configured to cooperatively control the gas flow into and out of the vaporisation chamber 9 so as to maintain the gas therein at the desired overpressure.

In one embodiment, the inlet valve 26 is controlled based on the pressure in the vaporisation chamber 9, while the outlet valve 17 is controlled based on pressure and/or flow measurements obtained downstream of the vaporisation chamber 9 and indicative of the respiratory phase of the patient 2. Preferably, the outlet valve 17 is controlled to deliver a varying flow of gas from the vaporisation chamber 9, which flow is adapted to the respiration cycle of the patient 2, and the inlet valve 26 is controlled so as to maintain the pressure in the vaporisation chamber 9 between a minimum pressure threshold value and a maximum pressure threshold value.

The minimum pressure threshold value is selected such that a sufficient flow of gas can be delivered from the vaporisation chamber 9 during inspiration phases of the patient 2. To this end, the minimum pressure threshold value is preferably selected such that the desired flow profile can be delivered to the patient via the outlet valve 17 during inspiration of the patient 2. In order to maintain the pressure in the vaporisation chamber 9 above said minimum pressure threshold value throughout the inspiration phases of the patient, the flow regulating means 17, 25, 26 controls the inflow and outflow into and out of the vaporisation chamber 9 to obtain a pressure corresponding to the maximum pressure threshold value in the vaporisation chamber 9 during expiration of the patient. The maximum pressure threshold value should be reached at least at the end of each expiratory phase, and so corresponds to an end-expiratory target pressure in the vaporisation chamber. This maximum pressure/end-expiratory target pressure is selected such that too high flows of gas to the patient 2 is avoided even if the outlet valve 17 should go from a closed position to a fully open position at said pressure. However, it should be selected high enough to ensure that a sufficiently high flow and volume of vapour-containing gas can be delivered to the patient 2 during the

following inspiration. The maximum pressure threshold value and the dynamics of the outlet valve 17 set an upper limit for the flow of vapour-containing gas that can be delivered to the patient 2.

During expiration phases of the patient, the outlet valve 17 is preferably controlled to fully quench the flow of vapour-containing gas out of the vaporisation chamber 9, while the inlet valve 26 is controlled to obtain the end-expiratory target pressure in the vaporisation chamber. The outlet valve 17 may also be controlled such that a low bias flow of vapour-containing gas is delivered to the patient 2 from the vaporisation chamber 9 during expiration phases. During inspiration phases of the patient 2, the outlet valve 17 is opened and regulated such that the overpressure in the vaporisation chamber 9 causes a desired flow of vapour-containing gas to leave the vaporisation chamber through the gas outlet channel 18. The inlet valve 26 may be closed during inspiration of the patient 2. In some embodiments, however, the inlet valve 26 may be open during the whole or parts of the inspiration phase, and regulated so as to maintain the pressure in the vaporisation chamber 9 above the minimum pressure threshold value.

In some embodiments, the inlet valve 26 and the outlet valve 17 of the vaporiser arrangement 7A may hence be controlled such that they are never open simultaneously, in order for the vaporisation chamber 9 to serve as a gas lock wherein the gas is maintained at an overpressure between the minimum and maximum pressure threshold values.

The outlet valve 17 may be controlled to deliver a constant flow of vapour-containing gas during the inspiration phase of the patient, or it may be controlled to deliver a flow that varies during the inspiration phase based on measured and/or preset parameters.

The capability of delivering a controlled and varied flow during inspiration phases is advantageous in that the flow of vapour-containing gas from the vaporisation chamber 9 can be adjusted to deliver a preset tidal volume to

the patient 2, or to maintain a preset proximal pressure in the breathing circuit, substantially corresponding to the airway pressure of the patient 2. Compared to a conventional fresh gas vaporiser which is a passive component through which the carrier gas passes freely, this makes the vaporiser arrangement 7A an active, flow regulating component that can take over some or all of the functionality normally provided for by the drive unit 3 of the breathing apparatus.

Fig. 3 illustrates an example of a breathing apparatus 1B according to another embodiment of the invention.

In contrast to the vaporiser arrangement of the breathing apparatus 1A in Fig. 1, the vaporiser arrangement 7A is here intended and configured to deliver the entire tidal volume of breathing gas to the patient 2 during inspiration.

With simultaneous reference now made to Figs. 2 and 3, this means that the volume of the vaporisation chamber 9 and the overpressure at which the gas is maintained in the vaporisation chamber 9 preferably are selected such that the vaporiser arrangement 7A is capable of delivering at least 600 ml of vapour-containing gas during an inspiration phase of the patient 2, substantially corresponding to a tidal volume of an adult patient with normal lung capacity. Also, the gas flow regulation means is configured to deliver vapour-containing gas from the vaporisation chamber 9 at a flow that is maintained over 120 lpm during the entire inspiration phase of the patient 2.

The volume of the vaporisation chamber 9 and the overpressure at which the gas is maintained in the vaporisation chamber are important design parameters in order to deliver the desired flow and volume of vapour-containing gas from the vaporisation chamber 9 during an inspiration phase. A vaporisation chamber volume of 500 ml is sufficient to deliver 1000 ml of vapour-containing gas during an inspiration phase without the need for opening the inlet valve 26 to refill the vaporisation chamber 9 with carrier gas during said inspiration phase, if the pressure in the vaporisation chamber is 4

bar at the end of expiration (i.e. at start of inspiration) and 2 bar at the end of inspiration. If the pressure in the vaporisation chamber 9 goes from 2 bar to 1 bar during inspiration, the volume of the vaporisation chamber should be at least 1000 ml to deliver the same volume of gas, and if it goes from 1 bar to 0,5 bar, the volume of the vaporisation chamber 9 should be at least 2000 ml. Also, the dynamics of the outlet valve 17 should be adapted to the pressure range of the vaporisation chamber in order to deliver the desired flow of vapour-containing gas to the patient 2.

Fig. 4 illustrates an example of a breathing apparatus 1C according to yet another embodiment of the invention. Just like the breathing apparatus 1B in Fig. 3, the breathing apparatus 1C comprises a vaporiser arrangement 7B configured to deliver the entire tidal of breathing gas to the patient 2. In this embodiment, however, not only does the vaporiser arrangement 7B serve as a combined vaporiser and pressurised supply of vapour-containing gas for direct delivery to the patient 2, it also serves as a gas mixing chamber.

With simultaneous reference now made to Fig. 5 which shows the vaporiser arrangement 7B in greater detail, the breathing apparatus 1C is configured to deliver different pressurised carrier-gas components to a plurality of gas inlet channels 10A-10C of the vaporiser arrangement 7B. The carrier-gas components are preferably two or more in the group consisting of air, oxygen and nitrous oxide.

The gas flow regulating means of the vaporiser arrangement 7B comprises a controllable inlet valve 26A-C in the respective gas inlet channel 10A-10C, each controlled by a control unit of the vaporiser arrangement 7B or the breathing apparatus 1C based on measured and/or preset parameters. The controllable inlet valves 26A-C and the outlet valve 17 cooperatively control the gas flow into and out of the vaporisation chamber 9 so as to maintain the gas therein at the desired overpressure.

Also, the inlet valves 26A-C are controlled in dependence of each other so as to obtain a desired carrier gas mixture within the vaporisation chamber 9. To this end, the inlet valves 26A-C may be controlled based on both the pressure within the vaporisation chamber 9 and the composition of the gas within the vaporisation chamber or downstream of the vaporisation chamber 9, which may be measured by means of the gas analyser 19.

It should be appreciated that the inlet valves 26A-C and the outlet valve 17 are configured to cooperatively control the flow of gas into and out of the vaporisation chamber in the way described above with reference to the single inlet valve and the outlet valve of the vaporiser arrangement 7A in Fig. 2. Likewise, the discussion on the volume of the vaporisation chamber 9, the minimum and maximum pressure threshold values etc. also applies to the vaporiser arrangement 7C of this embodiment.

Fig. 6 illustrates yet another embodiment of a vaporiser arrangement 7C according to the invention. In contrast to the previously described vaporiser arrangements 7A, 7B being injection vaporisers, the vaporiser arrangement 7C is a flow-by vaporiser for vaporisation of a liquid 27. The vaporiser arrangement 7C may be an anaesthetic vaporiser in which case the liquid 27 is liquid anaesthetic or a humidifier in which case the liquid is water.

The major difference between this vaporiser arrangement 7C and the vaporiser arrangement 7B in Fig. 5 is that this vaporiser arrangement 7C comprises a receptacle 12C for the liquid 27 to be vaporised instead of an injection arrangement. The temperature of the liquid 27 is controlled through the supply of heat by means of the heat generating means 14 such that the liquid passively vaporises into the gas that is maintained in the vaporisation chamber 9. In this embodiment, the liquid receptacle 12B is formed by a lower portion of the vaporisation chamber 9, arranged to receive and retain liquid. Furthermore, the liquid inlet 11 of the vaporiser arrangement is arranged in an upper portion of the vaporisation chamber 9 such that the receptacle 12C can be refilled via the liquid inlet.

Besides the above differences, it should be appreciated that the vaporiser arrangement 7C is arranged as the vaporiser arrangement 7B described above with reference to Fig. 5.

Flow Control in Pressurised Gas Tank

- 5 While the above description relates to a new type of vaporiser arrangement where vaporisation takes place in a pressurised gas tank, the following description relates to pressurised gas tanks in general.

Pressurised gas tanks are often used in breathing apparatuses for mixing and/or storage of breathing gases that are to be delivered to a patient. An
10 example of a breathing apparatus comprising such a gas tank is disclosed in U.S. Patent No. 5,299,568.

In gas tank arrangements according to prior art, the outlet valve controlling the flow of gas out of the tank and towards the patient function as a conventional inspiration valve and is controlled based on pressure and/or
15 flow measurements obtained downstream of the outlet valve, and preset ventilation parameters set by the operator of the breathing apparatus.

To avoid too high flows and pressures of gas from the gas tank to the patient, breathing apparatuses with pressurised gas tanks normally comprises a safety relief valve downstream of the outlet valve of the gas tank for venting
20 breathing gas out of the system in case of too high pressure in the breathing circuit. The safety relief valve is controlled based on pressure measurements obtained downstream the outlet valve of the gas tank.

To avoid the situation where breathing gas must be vented out of the system through a safety relief valve, it is suggested, according to one aspect of the
25 present invention, that the outlet valve that controls the flow of gas out of the gas tank is controlled based on the pressure within the gas tank.

Fig. 7 illustrates a gas tank arrangement 27 according to this aspect of the invention. The gas tank arrangement 27 comprises a gas tank 28, at least

one inlet valve 29A-C for controlling a flow of gas into said gas tank via at least one gas inlet channel 30A-C, and an outlet valve 31 for controlling the flow of gas out of the gas tank 28 and towards a patient via a gas outlet channel 32.

- 5 It should be appreciated that the gas tank arrangement 27 is intended to be used in a breathing apparatus, such as the breathing apparatus 1C in Fig. 4, in which it may replace the vaporiser arrangement 7B.

Preferably, the gas tank 28 serves as a mixing chamber in which two or more gas components such as air, oxygen and nitrous oxide, are mixed to form a
10 breathing gas that is to be delivered to a patient. To this end, the gas tank arrangement 27 may comprise two or more inlet valves 29A-C for controlling the flow of two or more gas components into the gas tank 28. It should, however, be appreciated that the gas components could also be mixed upstream of the gas tank arrangement 27 and that the gas mixture could be
15 delivered to the mixing chamber through a single inlet channel 30A under the control of a single inlet valve 29A of the gas tank arrangement.

The gas tank arrangement 27 may further comprise a flush outlet 33 for flushing gas out of the gas tank 28 via a flush outlet channel, and a flush valve 34 for controlling the flow of gas out of the gas tank 28 through said
20 flush outlet 33.

The gas tank arrangement further comprises a control unit 35 which is configured to control the at least one inlet valve 29A-C and the outlet valve 31 to maintain the gas within the gas tank 28 at an overpressure for subsequent delivery to the patient. The control unit 35 is configured to control
25 the at least one inlet valve 29A-C and the outlet valve 31 of the gas tank arrangement 27 such that they cooperatively control the flow of gas into and out of the gas tank 28 in the way the at least one inlet valve 26, 26A-26C and the outlet valve 17 control the flow of gas into and out of the vaporisation

chamber 9 of the vaporiser arrangements 7A-7C, described above with reference to Figs. 1 to 6.

It should be appreciated that the discussion on the volume of the vaporisation chamber 9 and the minimum and maximum threshold values for the
5 overpressure within the vaporisation chamber 9, discussed above with reference to Fig. 2, also applies to the volume of the gas tank 28 and the regulation of the overpressure therein.

Besides being configured to control the at least one inlet valve 29A-C and the outlet valve 31 as previously described, the control unit 35 is further
10 configured to control the outlet valve 31, and hence the flow of gas out of the gas tank 28, based on the pressure within the gas tank.

That the outlet valve 31 is controlled based on the pressure within the gas tank 28 means that the gas tank pressure is used by the control unit 35 as a variable in the control function for controlling the outlet valve 31. The
15 pressure in the gas tank may be obtained directly from a pressure sensor 36 in the gas tank, or it may be calculated from other measured parameters, such as the flow of gas into and out of the gas tank, measured by flow sensors 37A-C, 38A in the gas inlet channel(s) 30A-C and the gas outlet channel 32, and additionally also a flow sensor 38B arranged in a flush outlet
20 channel.

Controlling the outlet valve 31 based on the pressure in the gas tank 28 has the effect of being able to prevent too high flows from ever being delivered from the gas tank since the flow through the valve can be predicted by the control unit 35 given the pressure in the gas tank 28 and the dynamics of the
25 outlet valve 31.

This eliminates the risk of delivering too high flows of breathing gas from the gas tank 28 towards the patient, and thus eliminates the need for venting breathing gas out of the breathing apparatus downstream of the gas tank arrangement 27.

It further has the effect of allowing the function of the outlet valve 31 to be adapted to the current gas tank pressure. This in turn allows relatively high flows to be delivered from the gas tank 28 even at low gas tank pressures since the dynamics of the outlet valve can be adapted to allow a higher
5 degree of opening of the valve at low pressures than at high pressures.

- In one embodiment, the control unit 35 is adapted to determine an allowable range of operation of the outlet valve 31 based on the gas tank pressure, and to control the outlet valve 31 to operate only within said allowable range. The range of operation here means the degree of opening of the outlet valve 31.
- 10 To this end, the control unit 35 may be configured to determine a maximum degree of opening of the outlet valve 31 which, under the prevailing pressure condition in the gas tank 28, corresponds to a certain maximum flow of gas out of the gas tank, and to control the outlet valve 31 such that it is never opened to a higher degree than said maximum degree of opening.
- 15 Preferably, the control unit 35 is adapted to determine the allowable range of operation based on the gas tank pressure and a parameter that is indicative of the lung capacity of the patient, such as a preset tidal volume of the patient, a preset minute ventilation of the patient, or a preset parameter indicating whether the patient is an adult or a child. This allows the maximum
20 flow of gas out of the gas tank 28 to be tailored to the currently ventilated patient.

- Even more preferably, the allowable range of operation of the outlet valve 31 is adaptive and the control unit configured to adapt it based on changes in the gas tank pressure. For example, the control unit 35 may be configured to
25 determine a first maximum degree of opening of the outlet valve which should apply to pressures within a first pressure range, and a second maximum degree of opening of the outlet valve 31 which should apply to pressures within a second pressure range. In this way, the maximum degree of opening of the outlet valve can be high at low pressures and low at high
30 pressures, which ensures that a sufficient flow of gas can be delivered at low

pressures and that too high flows are avoided at high pressures. From a safety point of view it is advantageous to decrease the maximum degree of opening of the outlet valve if an increase in gas tank pressure is detected.

Using a slightly different wording, the control unit 35 can, in this embodiment, be said to adapt the resolution of the outlet valve 31 to the pressure in the gas tank 28, such that flows within a desired range of flows can be delivered to the patient, even if the pressure in the gas tank 28 varies substantially. The desired range of flows may be determined based on the previously mentioned parameter that is indicative of the lung capacity of the patient.

10 The outlet valve 31 is preferably electronically controlled. In one embodiment the outlet valve is an electronically controlled solenoid valve. In this case the degree of opening of the solenoid valve depends on the magnitude of an applied control current, and the control unit 35 may be configured to determine a maximum value for the control current so as to set a maximum degree of opening of the outlet valve.

The above described feature of controlling the outlet valve 31 based on the pressure within the gas tank 28 is applicable also to the previously described vaporiser arrangements 7A-7C. Thus, it should be understood that the outlet valve 17 in Figs. 2, 5 and 6 also may be controlled based on the pressure within the vaporisation chamber 9.

Efficient Flushing of Gas Tank

When using pressurised gas tanks as described above, there is sometimes a need for flushing the gas out of the gas tank as quickly as possible. This may for example be the case when there is an urgent need to change from one breathing gas composition to another.

Therefore, most gas tank-equipped breathing apparatuses comprise a flush valve for flushing the gas out of the gas tank and into open air or a

scavenging system. This is typically achieved by closing the outlet valve of the gas tank arrangement and opening the flush valve while supplying a flow of flushing gas into the gas tank via the gas inlet channel. After a while, the flushing gas has replaced the previous gas in the gas tank. If flushing of the gas tank is made due to a desire to switch to another breathing gas composition, the "other" breathing gas composition is typically used as flushing gas.

However, the flushing procedure often takes too long time. Typically, a very large volume of flushing gas is required to flush a relatively small volume of gas out of the gas tank. How much flushing gas is required to flush a sufficiently large portion of the previous gas out of the gas tank depends on the flow of the flushing gas and, in particular, on the design of the gas tank..

A gas tank arrangement that solves or at least mitigates this problem will now be described with reference to Figs. 8 and 9.

Fig. 8 illustrates a gas tank arrangement 39A for a breathing apparatus, comprising a gas tank 40A, at least one inlet valve 41 for controlling a flow of gas into said gas tank 40A via a gas inlet channel 42, an outlet valve 43 for controlling the flow of gas out of said tank 40 and towards a patient via a gas outlet channel 44, and a flush valve 45 for enabling flushing of gas out of the gas tank 40A via a flush outlet channel 46.

Preferably, the gas tank 40A serves as a mixing chamber in which two or more gas components, such as air, oxygen and nitrous oxide, are mixed. To this end, the gas tank 40A may comprise two or more inlet valves for controlling the flow of two or more gas components into the gas tank 40A via two or more gas inlet channels, in accordance with the embodiment of the gas tank arrangement 27 illustrated in Fig. 7. In this embodiment, however, the gas tank arrangement 39A is seen to comprise a single inlet valve 41 and the gas components that form the breathing gas are premixed in a mixing

stage (not shown) upstream of the inlet valve 41 for further mixing in the mixing chamber constituted by the gas tank 40A.

It should be appreciated that the gas tank arrangement 39A is intended to be used in a breathing apparatus, such as the breathing apparatus 1C in Fig. 4,
5 in which it may replace the vaporiser arrangement 7B.

The at least one inlet valve 41 and the outlet valve 43 are configured to maintain the gas within the gas tank 40A at an overpressure for subsequent delivery to the patient. To this end, the at least one inlet valve 41 and the outlet valve 43 cooperatively control the flow of gas into and out of the gas
10 tank 40A in the way the at least one inlet valve 26, 26A-26C and the outlet valve 17 control the flow of gas into and out of the vaporisation chamber 9 of the vaporiser arrangements 7A-7C, described above with reference to Figs. 1 to 6.

It should be appreciated that the discussion on the volume of the vaporisation
15 chamber 9 and the minimum and maximum threshold values for the overpressure within the vaporisation chamber 9, discussed above with reference to Fig. 2, also applies to the volume of the gas tank 40A and the regulation of the overpressure therein.

As illustrated in the drawing, the gas tank 40A is elongated and at least one
20 of the at least one inlet valves 41 and the outlet valve 43 are arranged in opposite ends of the elongated gas tank 40A. The flush valve 45 is arranged in the same end as the outlet valve 43 so that gas can be efficiently pushed out of the gas tank 40A through the flush valve 45 by a flow of gas through the inlet valve 41 when the outlet valve 43 is closed. That the flush valve 45
25 is arranged in the same end as the outlet valve 43 means that it is arranged in the downstream-end of the elongated gas tank 40A.

For optimal flushing performance, the elongated gas tank 40A should be designed such that a well-defined front is formed between the gas that is to be flushed out of the gas tank 40A and the flushing gas that is supplied

through the inlet valve 41, so that a minimum of mixing occurs between the gas volumes. In this way, the ratio between the volume of flushing gas needed to flush a gas out of the gas tank 40A, and the volume of the gas to be flushed out of the tank becomes nearly 1:1.

- 5 Preferably, to obtain the effect of efficient pushing of the gas out of the gas tank, the elongated gas tank 40A is configured such that a laminar flow is created in the longitudinal direction of the elongated gas tank when the flushing gas flows through the gas tank 40A towards the flush valve 45. In order for such a laminar flow to occur, the length of the elongated gas tank
- 10 40A should preferably be at least ten times the width of the gas tank (i.e. the diameter of the gas tank in case the tank has a circular cross-section).

Preferably, the maximum width of the tank is between 1 and 10 cm, and even more preferably between 3 and 7 cm. The elongated gas tank 40A is preferably a cylindrical gas tank in which case said maximum width

15 corresponds to the diameter of the gas tank

Even more preferably, the elongated gas tank 40A has a length of at least 60 cm and a width or diameter of at most 6 cm.

- The gas tank 40A may further comprise local turbulence generating means (not shown) for generating a local turbulence in the gas tank. This is
- 20 advantageous in that a laminar flow can be achieved in the gas tank even at a relatively short distance from the inlet of the gas tank (substantially shorter than 10 times the width of the gas tank), which further improves the effect of pushing the gas out of the gas tank. An additional effect of the local turbulence generating means is hence that the elongated gas tank 40A can
- 25 be made shorter than 10 times its width while still allowing a laminar flow to occur in the tank. To obtain the laminar flow as close to the inlet of the gas tank 40A as possible, the local turbulence generating means is preferably arranged close to the inlet end of the elongated gas tank 40A, i.e. the end of the gas tank in which the inlet valve 41 is arranged.

Preferably, the local turbulence generating means is arranged to generate local turbulence along a direction that is substantially perpendicular to the longitudinal direction of the elongated gas tank. To this end, the local turbulence generating means may comprise one or more elements arranged
5 in said plane. Preferably it comprises a plurality of elongated members arranged in said plane. In one embodiment, the local turbulence generating means comprises a net arranged in a plane that is substantially perpendicular to the longitudinal direction of the elongated gas tank. The net should preferably be arranged in the inlet end of the gas tank 40A.

10 Preferably, the volume of the elongated gas tank 40A is at least 500 ml, more preferably at least 1000 ml, and even more preferably at least 2000 ml.

The principle used to push the gas out of the gas tank is the same principle used in what is often referred to as a volume reflector, in which gases exhaled by the patient are collected in a hose and pushed back to the patient
15 by a drive gas that is supplied through a distal end of the hose. Sometimes such volume reflectors are referred to as a Werner volumes after the inventor of U.S. Patent No. 4,989,597 where the principle was first described.

The gas tank may be a straight tubular gas tank as illustrated in Fig. 8 but the demands on the volume and the cross section of the gas tank may, in view of
20 other design requirements of the breathing apparatus of which it forms a part, require the elongated gas tank to be curved. Therefore, in some embodiments, the gas tank may be formed as a curved elongated gas flow channel. The volume of the gas flow channel should preferably be 1000 ml or more, and even more preferably 2000 ml or more.

25 Fig. 9 illustrates an exemplary embodiment of a gas tank arrangement 39B comprising a gas tank 40B in form of a curved elongated gas channel. In this embodiment, the curved elongated gas channel forming the gas tank 40B is spiral-shaped and enclosed in a gas tank housing 47.

It should be appreciated that the vaporiser arrangement 7A, 7B, 7C described above with reference to Figs. 1-6 also may be designed as described in this section in order to achieve the effect of more efficient flushing of vapour-containing carrier gas out of the vaporisation chamber 9.

CLAIMS

1. A vaporiser arrangement (7) for a breathing apparatus (1), comprising :
 - at least a first gas inlet channel (10) for conveying a flow of a carrier gas into a vaporisation chamber (9);
 - 5 - vaporisation means (12) for vaporising a liquid into the carrier gas in the vaporisation chamber, and
 - a gas outlet channel (18) for conveying a flow of vapour-containing carrier gas out of the vaporisation chamber and towards a patient (2),
 - 10 **characterised in** that the vaporiser arrangement (7) further comprises gas flow regulating means (17, 25, 26) configured to maintain the carrier gas within the vaporisation chamber (9) at an overpressure, and to control the flow of vapour-containing carrier gas out of the vaporisation chamber in a variable manner.
- 15 2. Vaporiser arrangement (7) according to claim 1, wherein the gas flow regulating means (17, 25, 26) is configured to control the flow of vapour-containing carrier gas out of the vaporisation chamber (9) based on at least one parameter indicative of the respiratory phase of the patient.
- 20 3. Vaporiser arrangement (7) according to any of the preceding claims, wherein the gas low regulating means (17, 25, 26) further is configured to control the flow of carrier gas into the vaporisation chamber in a variable manner.
- 25 4. Vaporiser arrangement (7) according to claim 3, wherein the gas flow regulating means (17, 25, 26) is configured to control the flow of carrier gas into the vaporisation chamber (9) based on measurements (P , ϕ_{i1} , ϕ_{i2} , ϕ_{i3} , ϕ_{f1}) indicative of the pressure within the vaporisation chamber (9).

5. Vaporiser arrangement (7) according to claim 3 or 4, wherein the gas flow regulating means (17, 25, 26) is configured to always maintain the pressure in the vaporisation chamber (9) between a minimum pressure threshold value and a maximum pressure threshold value.
- 5
6. Vaporiser arrangement (7) according to claim 5, wherein the minimum and/or maximum pressure threshold value is determined based on preset parameters relating to:
- the tidal volume of the patient,
 - 10 - the dynamics of an outlet valve (17) for controlling the flow of vapour-containing gas out of the vaporisation chamber (9), and/or
 - a minimum and/or maximum flow of vapour-containing gas out of the vaporisation chamber (9).
- 15 7. Vaporiser arrangement (7) according to claim 5, wherein the gas flow regulating means (17, 25, 26) further is configured to maintain the pressure in the vaporisation chamber (9) at an end-expiratory target pressure at the end of each expiratory phase of the patient, which end-expiratory pressure corresponds to said maximum pressure threshold
- 20 value.
8. Vaporiser arrangement (7) according to any of the claims 3 to 7, wherein the gas flow regulating means (17, 25, 26) is configured to, at least during an initial phase of an inspiration phase of the patient (2), prevent flow of
- 25 carrier gas into the vaporisation chamber (9).
9. Vaporiser arrangement (7) according to claim 8, wherein the gas flow regulating means (17, 25, 26) is configured to, during a final phase of said inspiration phase, provide a flow of carrier gas into the vaporisation
- 30 chamber (9) and control said flow so as to maintain the overpressure over a certain minimum pressure threshold value.

10. Vaporiser arrangement (7) according to any of the claims 3 to 9, wherein the gas flow regulating means (17, 25, 26) is configured to prevent simultaneous flow of carrier gas into the vaporisation chamber (9) and flow of vapour-containing gas out of the vaporisation chamber (9).
- 5
11. Vaporiser arrangement (7) according to any of the preceding claims, wherein the volume of the vaporisation chamber (9) and said desired overpressure are selected such that at least 600 ml of gas can be delivered from the vaporisation chamber (9) at a flow that never falls
- 10 below 120 lpm during an inspiration phase of the patient.
12. Vaporiser arrangement according to any of the previous claims, wherein the gas flow regulating means (17, 25, 26) comprises a controllable outlet valve (17) for controlling the flow of vapour-containing carrier gas out of
- 15 the vaporisation chamber (9).
13. Vaporiser arrangement according to any of the claims 3 to 12, wherein the gas flow regulating means (17, 25, 26) comprises a controllable inlet valve (17) for controlling the flow of carrier gas into the vaporisation
- 20 chamber (9).
14. Vaporiser arrangement (7) according to any of the preceding claims, further comprising at least a second gas inlet channel (26) for introducing at least a second gas into the vaporisation chamber (9) so as to allow
- 25 said first and at least second gas to mix within the vaporisation chamber to form said carrier gas.
15. Vaporiser arrangement (7) according to claim 14, wherein the gas flow regulating means (17, 25, 26) is configured to control the flow of gas
- 30 through the respective gas inlet channel (26) so as to obtain a desired carrier gas mixture in the vaporisation chamber.

16. Vaporiser arrangement according to any of the preceding claims, wherein said liquid is an anaesthetic agent or water.
17. A breathing apparatus (1) for providing breathing support to a patient (2),
5 **characterised in** that the breathing apparatus comprises a vaporiser arrangement (7) according to any of the previous claims.
18. Breathing apparatus (1) according to claim 17, wherein said vaporiser arrangement (7) is an anaesthetic vaporiser for vaporisation of liquid
10 anaesthetic.
19. Breathing apparatus (1) according to claim 17, wherein said vaporiser arrangement (6) is a humidifier for vaporisation of water.
- 15 20. Breathing apparatus (1) according to any of the claims 17 to 19, wherein the breathing apparatus is arranged to deliver the entire volume of breathing gas to the patient (2) during inspiration from said vaporiser arrangement (7).
- 20 21. A gas tank arrangement (27) for a breathing apparatus, comprising:
 - a gas tank (28),
 - an inlet valve (29) for controlling a flow of gas into said gas tank,
 - an outlet valve (31) for controlling the flow of gas out of said gas tank and towards a patient, and
25 - a control unit (35) for controlling said inlet and outlet valves to maintain the gas within said gas tank at an overpressure for subsequent delivery to the patient,
 characterised in that the control unit (35) is configured to control the outlet valve (31) based on a parameter that is indicative of the pressure
30 within the gas tank (28).

22. A gas tank arrangement (27) according to claim 21, wherein the control unit (35) is adapted to determine an allowable range of operation of said outlet valve (31) based on said parameter, and to control the outlet valve to operate only within said allowable range.

5

23. A gas tank arrangement (27) according to claim 22, wherein the control unit (35) is adapted to determine said allowable range of operation of the outlet valve (31) based on said parameter and a second parameter indicative of the lung capacity of the patient.

10

24. A gas tank arrangement (27) according to claim 22 or 23, wherein said allowable range of operation of the outlet valve (31) is adaptive, and said control unit (35) is configured to adapt the allowable range of operation of the outlet valve based on changes in the gas tank pressure.

15

25. A gas tank arrangement (27) according to claim 24, wherein the control unit (35) is configured to decrease the allowable range of operation of the outlet valve based on an increase in the gas tank pressure.

20

26. A gas tank arrangement (27) according to any of the claims 22 to 25, wherein the outlet valve (31) is electronically controlled, and wherein the degree of opening of the outlet valve depends on a control current supplied to the outlet valve, the control unit (35) being configured to determine said allowable range of operation of the outlet valve (31) by determining a maximum value for said control current.

25

27. A gas tank arrangement (27) according to any of the claims 21 to 26, wherein said parameter indicative of the pressure within the gas tank (28) is obtained by a pressure sensor (36) in the gas tank or by flow

30

sensors (37, 38) arranged to measure the flow of gas into and out of the gas tank.

28. A gas tank arrangement (27) according to any of the claims 21 to 27,
5 wherein the gas tank (28) forms a mixing chamber for two or more gas components forming a breathing gas mixture that is to be supplied to the patient.
29. A gas tank arrangement (27) according to claim 28, further comprising a
10 gas mixing stage for mixing two or more gas components to be delivered to the gas tank (28), upstream of said inlet valve (29).
30. A gas tank arrangement (27) according to claim 28, wherein said inlet
15 valve (29) controls the flow of a first gas component into the gas tank (28), the gas tank arrangement further comprising a second inlet valve (29) for controlling the flow of a second gas component into the gas tank.
31. A gas tank arrangement (39) for a breathing apparatus, comprising:
20 - a gas tank (40),
- an inlet valve (41) for controlling a flow of gas into said gas tank,
- an outlet valve (43) for controlling the flow of gas out of said gas tank, towards a patient, and
- a flush valve (45) for enabling flushing of gas out of said gas tank,
25 wherein said inlet and outlet valves are operable to maintain the gas within said tank at an overpressure for subsequent delivery to the patient,
characterised in that the gas tank (40) is elongated, **in that** the inlet valve (41) and the outlet valve (43) are arranged in opposite ends of the elongated gas tank (40), **and in that** the flush valve (45) is arranged in
30 the same end as the outlet valve (43) so that gas can be pushed out of the gas tank (40) through the flush valve (43) by a flow of gas supplied to the gas tank through the inlet valve (41), when the outlet valve (43) is closed.

32. A gas tank arrangement (39) according to claim 31, wherein said elongated gas tank (40) has a length that is at least ten times its width.

5 33. A gas tank arrangement (39) according to claim 31 or 32, wherein the elongated gas tank (40) comprises local turbulence generating means for generating local turbulence within the gas tank (40).

10 34. A gas tank arrangement (39) according to claim 32, wherein said local turbulence generating means comprises one or more elements arranged in a plane that is substantially perpendicular to the longitudinal direction of the elongated gas tank (40).

15 35. A gas tank arrangement (39) according to claim 34, wherein said local turbulence generating means is a net.

20 36. A gas tank arrangement (39) according to any of the claims 31 to 35, wherein a maximum width or diameter of the elongated gas tank (40) is between 1 and 10 centimetres.

25 37. A gas tank arrangement (39) according to any of the claims 31 to 36, wherein said gas tank forms an elongated gas flow channel between said inlet (41) and said outlet (43), said gas flow channel being curved.

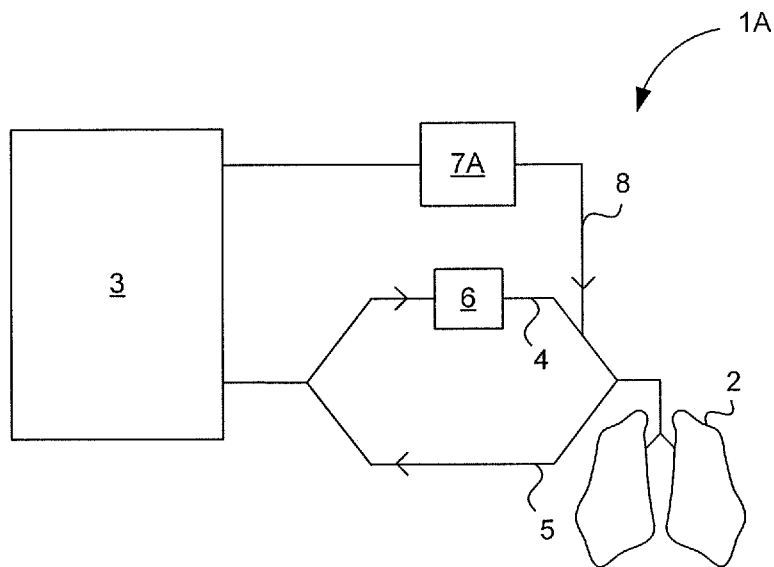


FIG 1

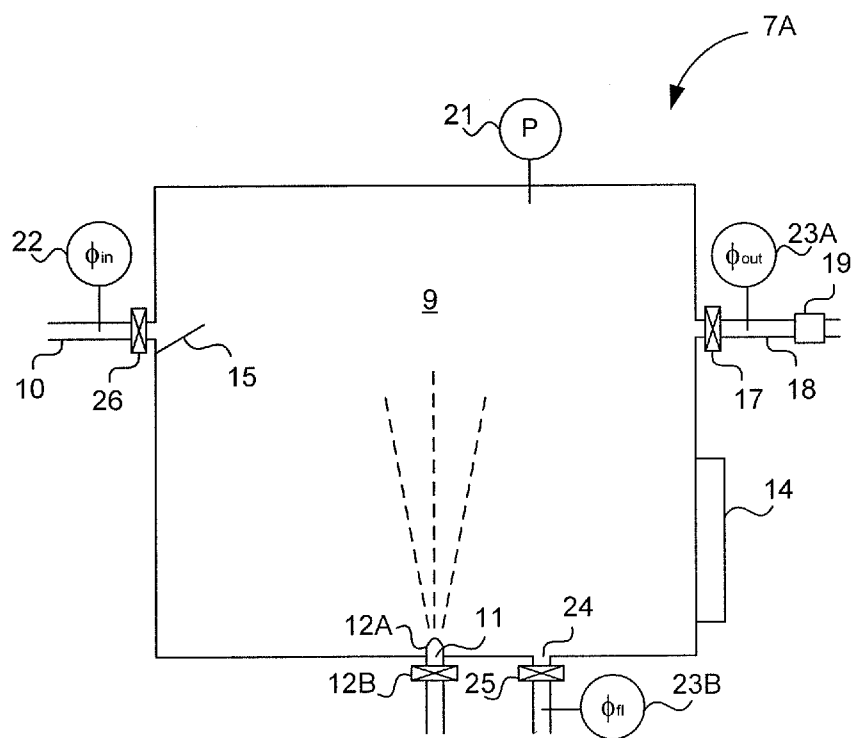
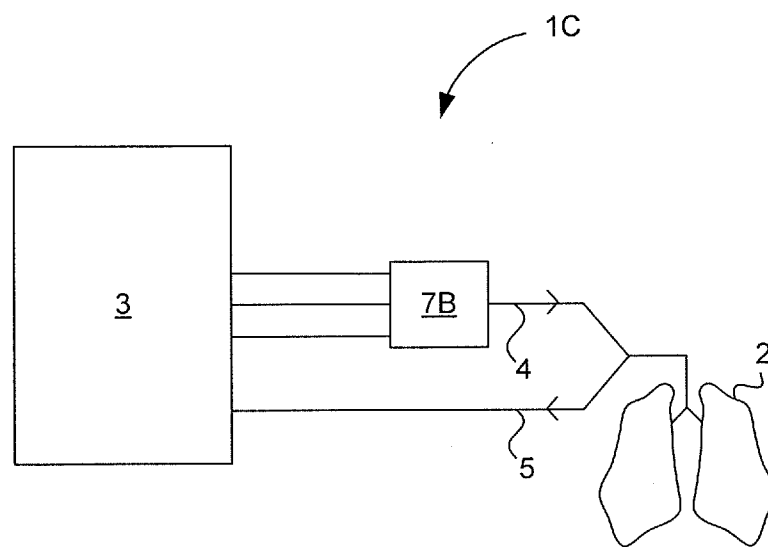
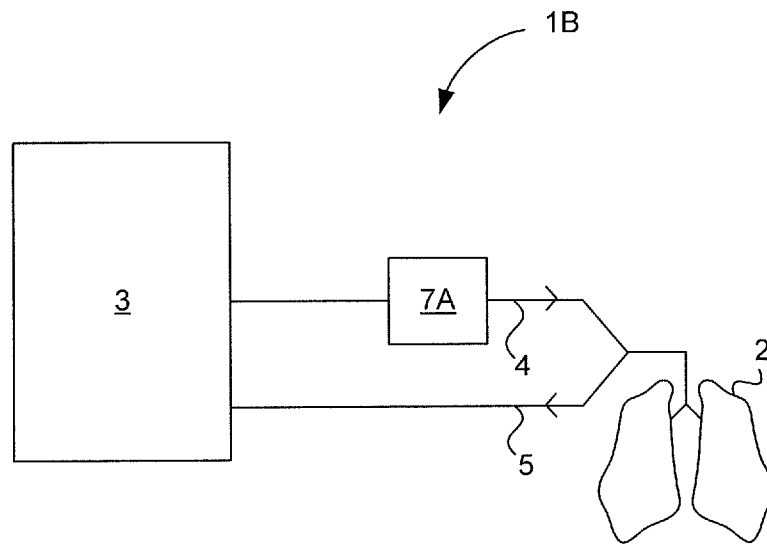
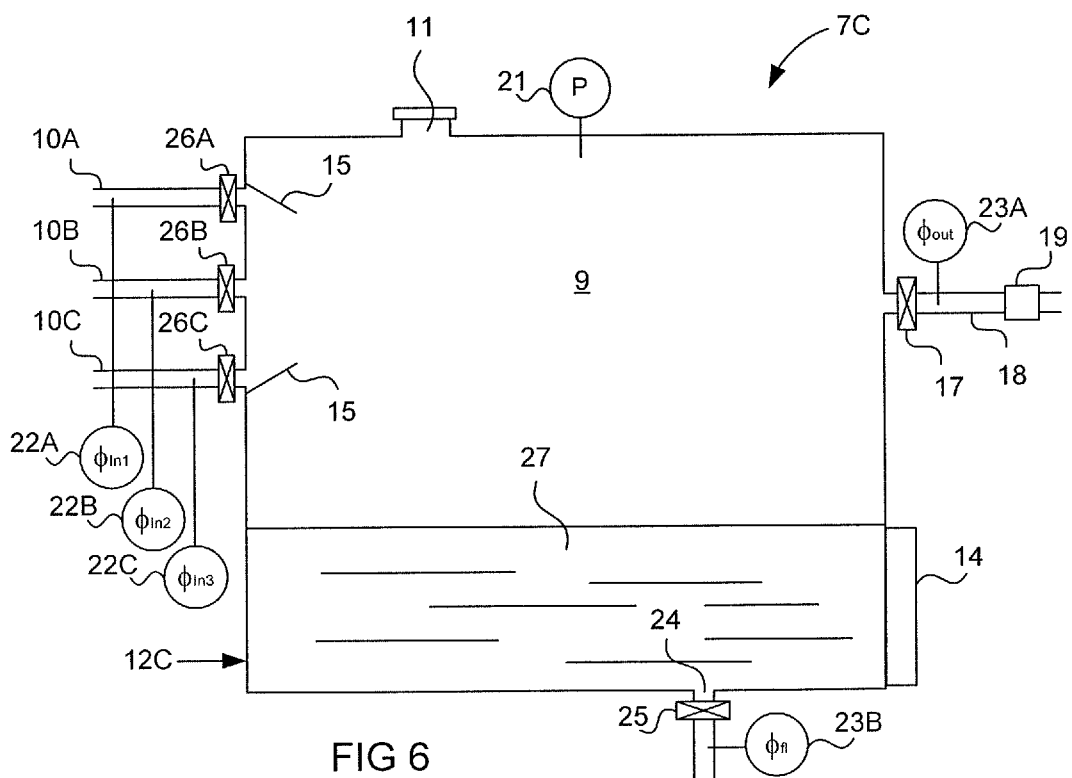
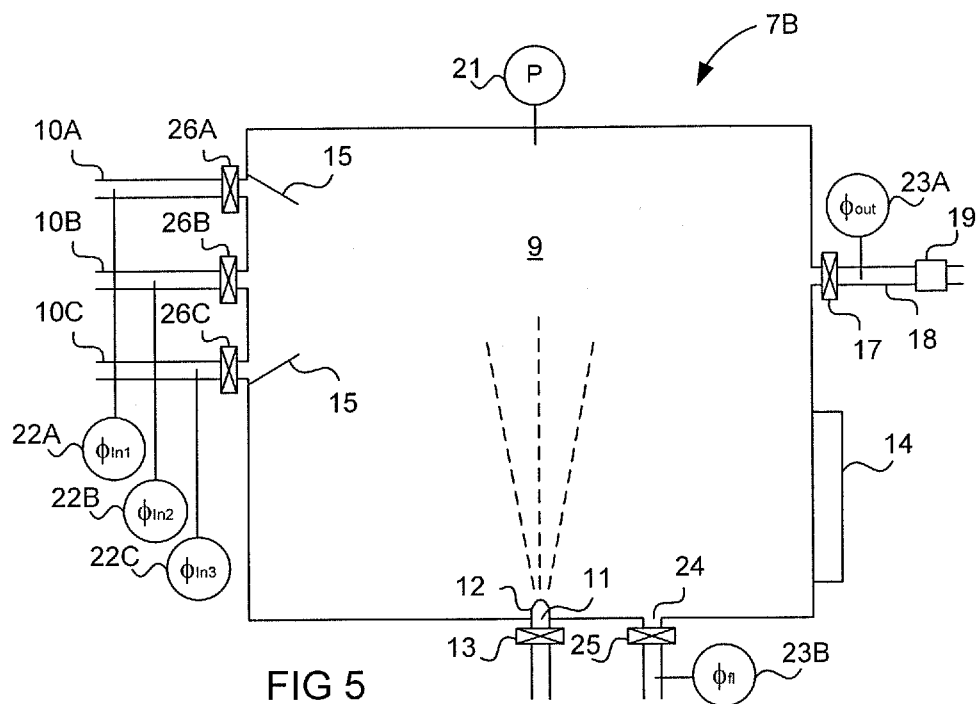


FIG 2





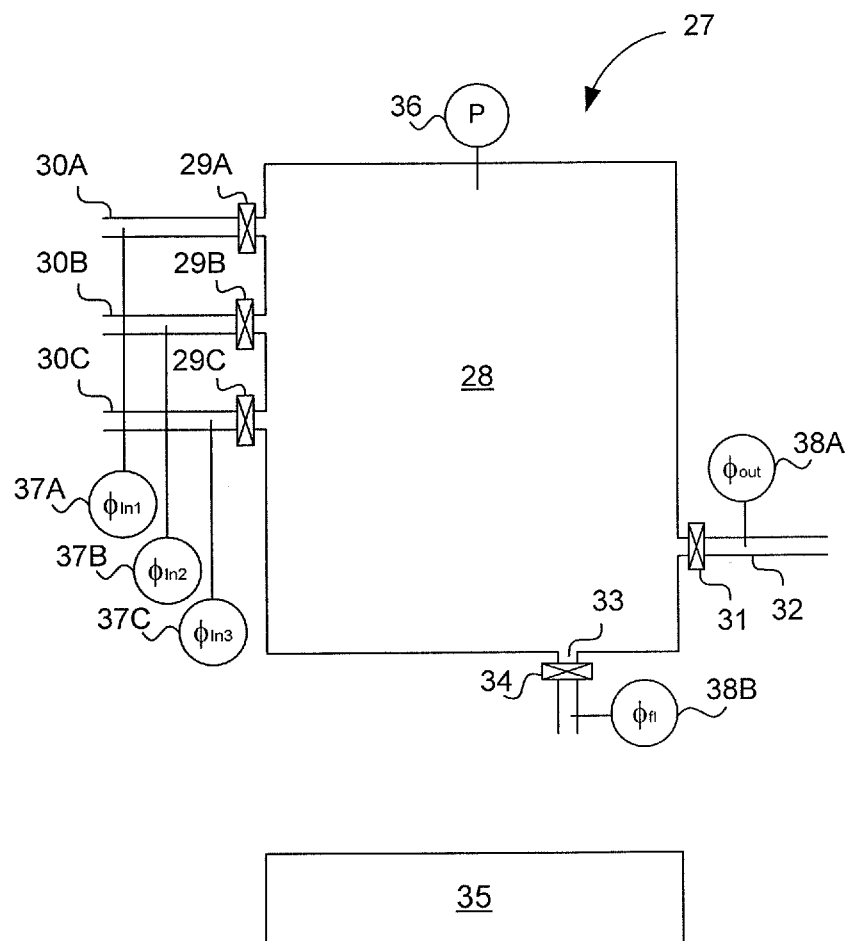


FIG 7

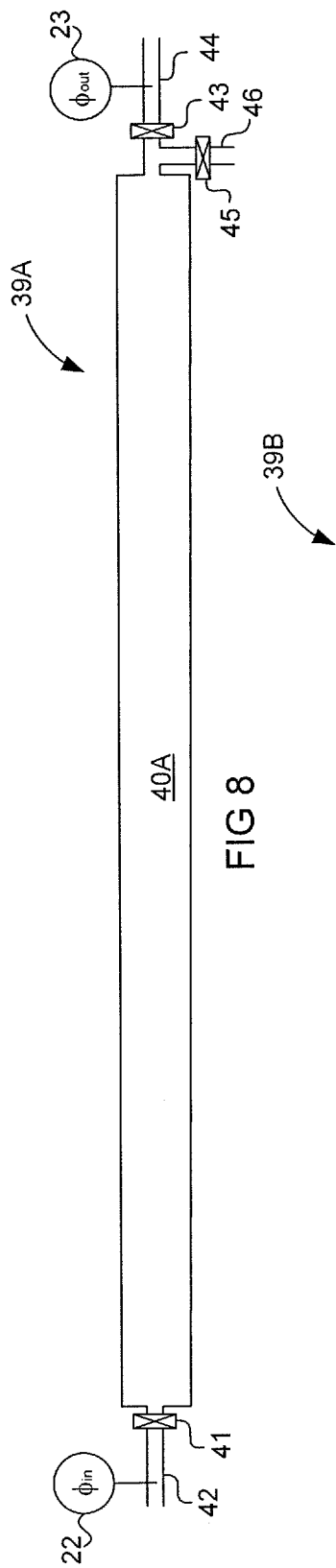


FIG 8

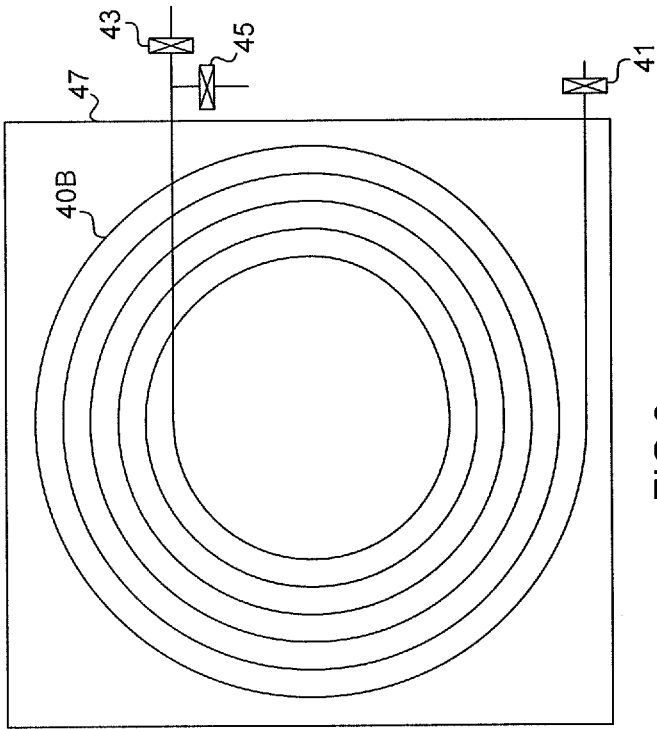


FIG 9

INTERNATIONAL SEARCH REPORT

International application No
PCT/SE2011/051597

A. CLASSIFICATION OF SUBJECT MATTER

INV. A61M16/10 A61M16/18 A61M16/12
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61M

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-Internal , WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	DE 41 05 971 A1 (DRAEGERWERK AG [DE]) 27 August 1992 (1992-08-27)	1,3-5 ,8, 9 , 11-13, 16-20
Y	col umn 2 , l ines 55-63	2
A	col umn 3 , l ines 31-40	6,7, 10,
	col umn 3 , l ine 60 - col umn 5 , l ine 34; figure 1	14, 15

Y	US 7 438 072 B2 (IZUCHUKWU JOHN I [US]) 21 October 2008 (2008-10-21)	2
	col umn 15 , l ine 5 - col umn 16 , l ine 42; figures 14, 14D	

A	EP 0 722 748 A2 (INSTRUMENTARIUM OY [FI] INSTRUMENTARIUM CORP [FI]) 24 July 1996 (1996-07-24)	1-20
	col umn 4 , l ine 13 - col umn 5 , l ine 11; figure 1	

	- / - -	



Further documents are listed in the continuation of Box C.



See patent family annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

28 November 2012

Date of mailing of the international search report

06/12/2012

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INTERNATIONAL SEARCH REPORT

International application No.
PCT/SE20 11/05 1597

Box No. II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☐ Claims Nos.:
because they relate to subject matter not required to be searched by this Authority, namely:

2. ☐ Claims Nos.:
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box No. III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

see additional sheet

1. ☒ As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.

2. ☐ As all searchable claims could be searched without effort justifying an additional fees, this Authority did not invite payment of additional fees.

3. ☐ As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos. :

4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest and, where applicable, the payment of a protest fee.
- ☐ The additional search fees were accompanied by the applicant's protest but the applicable protest fee was not paid within the time limit specified in the invitation.
- ☒ No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

International application No
PCT/SE2011/051597

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 4 023 587 A (DOBRITZ GUNTHER) 17 May 1977 (1977-05-17)	21, 27-30
Y	column 4, line 41 - column 5, line 18; figure 1 -----	22, 26
Y	US 2009/205661 A1 (STEPHENSON ROBERT [US] ET AL) 20 August 2009 (2009-08-20)	22, 26
A	paragraph [0026]; figure 1 paragraph [0039] -----	23-25, 31-37
E	EP 2 489 392 A1 (LINDE AG [DE]) 22 August 2012 (2012-08-22) paragraphs [0062], [0070], [0075] - [0078]; figure 2 -----	21-23, 26-30
A	US 2011/132364 A1 (OGILVIE MARK [US] ET AL) 9 June 2011 (2011-06-09) paragraphs [0060] - [0063]; figures 2c, 2d, 3 -----	31-37

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

This International Searching Authority found multiple (groups of) inventions in this international application, as follows:

1. claims: 1-20

A vaporiser arrangement comprising a vaporisation chamber and gas flow regulating means configured to maintain the carrier gas in the vaporisation chamber at an overpressure

2. claims: 21-30

A gas tank arrangement comprising a gas tank, an outlet valve and a control unit configured to control the outlet valve based on a parameter that is indicative of the pressure within the gas tank.

3. claims: 31-37

A gas tank arrangement comprising a gas tank, an outlet valve and a flush valve arranged on the same end as the outlet valve.

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/SE2011/051597

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
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			DE 69624734 T2 13-03-2003
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