

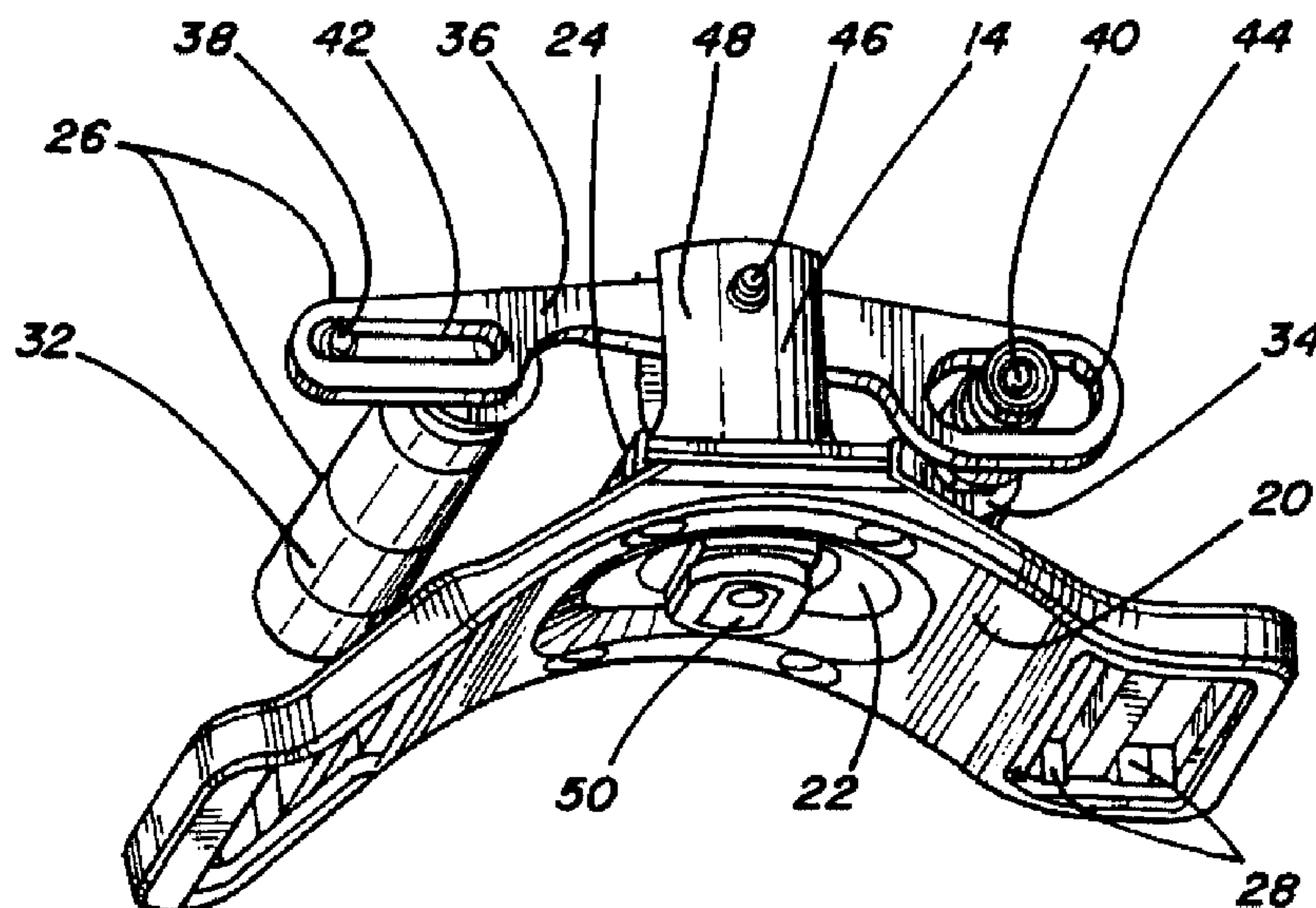


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(54) Titre : DISPOSITIF ET PROCEDE DE SURVEILLANCE NON INVASIVE DE LA PRESSION SANGUINE
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(54) Title: APPARATUS AND METHOD FOR NON-INVASIVELY MONITORING A SUBJECT'S ARTERIAL BLOOD
PRESSURE



(57) Abrégé/Abstract:

Apparatus is disclosed for non-invasively monitoring a subject's blood pressure, in which a pressure sensor assembly (14) that includes a pressure transducer (50) is compressed against tissue overlying an artery, with sufficient force to compress the artery. A motor (32) first servo control system optimizes the amount of artery compression, which occurs at a mean transmural pressure of about zero, by modulating one side of a lever arm (36) compressing the assembly against the tissue, creating a pressure signal indicative of transmural pressure. Since different pressure effects are realized according to the amount of artery compression, an appropriate control signal can be produced that provides for a second motor (34) to adjust the other side of the lever arm (36) to provide the optimum compression of the assembly into the tissue overlying the artery. The apparatus is optimally positioned over an artery by including an ultrasonic blood flow sensor configured to sense the flow of blood under the pressure transducer.





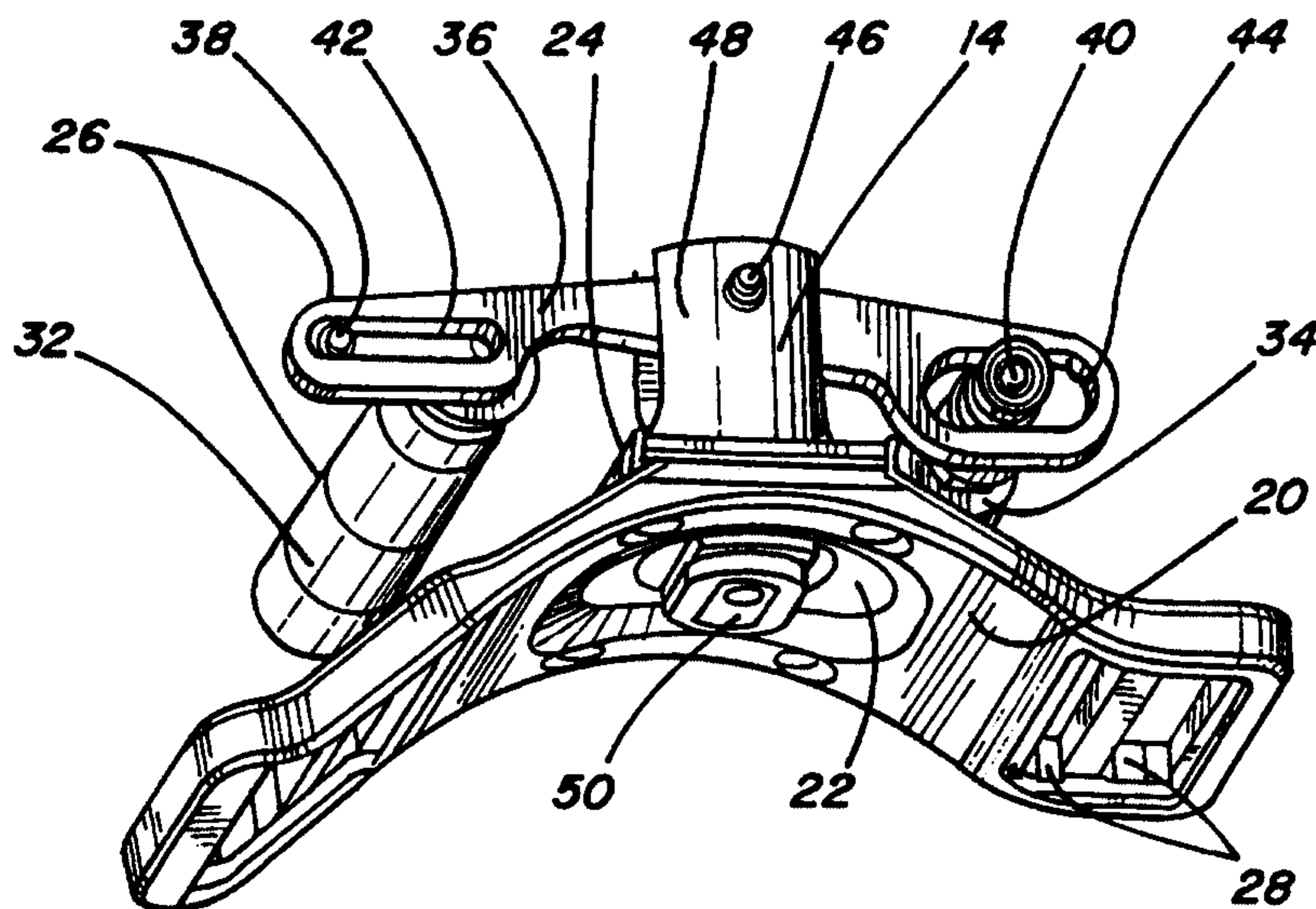
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(54) Title: APPARATUS AND METHOD FOR NON-INVASIVELY MONITORING A SUBJECT'S ARTERIAL BLOOD PRESSURE



(57) Abstract

Apparatus is disclosed for non-invasively monitoring a subject's blood pressure, in which a pressure sensor assembly (14) that includes a pressure transducer (50) is compressed against tissue overlying an artery, with sufficient force to compress the artery. A motor (32) first servo control system optimizes the amount of artery compression, which occurs at a mean transmural pressure of about zero, by modulating one side of a lever arm (36) compressing the assembly against the tissue, creating a pressure signal indicative of transmural pressure. Since different pressure effects are realized according to the amount of artery compression, an appropriate control signal can be produced that provides for a second motor (34) to adjust the other side of the lever arm (36) to provide the optimum compression of the assembly into the tissue overlying the artery. The apparatus is optimally positioned over an artery by including an ultrasonic blood flow sensor configured to sense the flow of blood under the pressure transducer.

APPARATUS AND METHOD FOR NON-INVASIVELY MONITORING A SUBJECT'S ARTERIAL BLOOD PRESSURE

BACKGROUND OF THE INVENTION

This invention relates generally to apparatus and methods for monitoring a subject's arterial blood pressure and, more particularly, to such apparatus and methods that monitor arterial blood pressure non-invasively by applying a pressure sensor against tissue overlying an arterial blood vessel, to partially applanate or compress the vessel.

5

Two well-known techniques have been used to non-invasively monitor a subject's arterial blood pressure waveform, namely, auscultation and oscillometry. Both techniques use a standard inflatable arm cuff that occludes the subject's brachial artery. The auscultatory technique determines the subject's systolic and diastolic pressures by
10 monitoring certain Korotkoff sounds that occur as the cuff is slowly deflated. The oscillometric technique, on the other hand, determines these pressures, as well as the subject's mean pressure, by measuring actual pressure changes that occur in the cuff as the cuff is deflated. Both techniques determine pressure values only intermittently, because of the need to alternately inflate and deflate the cuff, and they cannot replicate
15 the subject's actual blood pressure waveform. Thus, true continuous, beat-to-beat blood pressure monitoring cannot be achieved using these techniques.

Occlusive cuff instruments of the kind described briefly above generally have been effective in sensing long-term trends in a subject's blood pressure. However,
20 such instruments generally have been ineffective in sensing short-term blood pressure variations, which are of critical importance in many medical applications, including surgery.

One technique that has been used to provide information about short-term
25 blood pressure variations is called arterial tonometry. One device for implementing this

technique includes a rigid array of miniature pressure transducers that is applied against the tissue overlying a peripheral artery, e.g., the radial artery. The transducers each directly sense the mechanical forces in the underlying subject tissue, and each is sized to cover only a fraction of the underlying artery. The array is urged against the tissue, to
5 applanate the underlying artery and thereby cause beat-to-beat pressure variations within the artery to be coupled through the tissue to the transducers.

The rigid arterial tonometer described briefly above is subject to several drawbacks. First, its discrete transducers are relatively expensive and, because they are
10 exposed, they are easily damaged. In addition, the array of discrete transducers generally is not anatomically compatible with the continuous contours of the subject's tissue overlying the artery being sensed. This has led to inaccuracies in the resulting transducer signals. In addition, in some cases, this incompatibility can cause tissue injury and patient discomfort. Another drawback is that such rigid arterial tonometers
15 have failed to correct for signal artifacts that arise when the subject's arm is moved. This is a particular problem when the subject is exercising or otherwise ambulating.

Yet another drawback to the arterial tonometer described briefly above is its inability to continuously monitor and adjust the level of arterial wall compression to
20 an optimum level of zero transmural pressure. Generally, optimization of arterial wall compression has been achieved only by periodic recalibration. This has required an interruption of the patient monitoring function, which sometimes can occur during critical periods. This drawback is perhaps the most severe factor limiting acceptance of tonometers in the clinical environment.

25

Another device functioning similarly to the arterial tonometer includes a housing having a closed, liquid-filled chamber with one wall of the chamber defined by a flexible diaphragm. The device is applied against a subject's skin, with the flexible diaphragm pressed against the tissue overlying a peripheral artery, e.g., the radial artery,
30 and several electrodes located in separate compartments of the chamber sense volume

changes in the compartments that result from the beat-to-beat pressure variations in the underlying artery. Although the device seeks to replicate the arterial pressure waveform, it is considered to have a relatively low gain, making it unduly susceptible to noise. Further, the device must be calibrated periodically, during which time its continuous
5 monitoring of the subject's blood pressure waveform necessarily is interrupted.

It should, therefore, be appreciated that there is a continuing need for an apparatus, and related method, for non-invasively and continuously monitoring a subject's blood pressure, with reduced susceptibility to noise and without the need to
10 intermittently interrupt the device's normal operation for calibration. Various embodiments of the present invention can fulfill some or all of these requirements.

SUMMARY OF THE INVENTION

15 The present invention resides in an improved apparatus, and related method, for non-invasively monitoring a subject's arterial blood pressure, with reduced susceptibility to noise and without the need to intermittently interrupt the pressure monitoring for calibration. The apparatus includes a pressure transducer that produces a
20 pressure signal indicative of the pressure applied against it and further includes a coupling device that urges the pressure transducer into compressive association and engagement with tissue overlying the subject's blood vessel, to compress the vessel and ensure that pressure variations within the vessel are coupled through the tissue to the pressure transducer.

25 A controller controls the coupling device to controllably modulate the location of the pressure transducer relative to a nominal location that is static with respect to the subject's blood vessel. The controller also monitors the resulting effect of the modulation on the pressure signal, producing an error signal (i.e., a control signal)
30 that is indicative of the deviation of the nominal location from a preferred target

location. Preferably, the coupling device is configured to respond to the error signal by controllably adjusting the nominal location toward the target location. When the nominal location is at or substantially close to the target location, the blood vessel is compressed according to a prescribed requirement, which is preferably a prescribed mean amount providing a transmural pressure of substantially zero. This requirement optimizes the coupling between the blood vessel and the sensor assembly. The pressure sensor assembly thereby senses the subject's blood pressure in an optimal manner.

More particularly, in one form of the invention, the pressure sensor assembly includes a base configured to provide reaction forces for urging the pressure transducer into compressive association with the tissue overlying the subject's blood vessel. The coupling device includes a first variable positioning device, such as a first motor with an eccentric cam, configured to controllably adjust the nominal location toward the target location. The coupling device also includes a second variable positioning device, such as a second motor with an eccentric cam, configured to vary the pressure transducer through a range of locations relative to the nominal location, i.e., modulating the pressure transducer about the nominal location.

Preferably, the first and second variable positioning devices actuate a first and second end of a lever arm, respectively, to actuate the pressure transducer, which is connected to the lever arm between the two ends. By monitoring the effect on the pressure signal of the second variable positioning device, the controller can direct the first variable positioning device to adjust the lever arm such that the nominal location moves, and thus the subject's blood vessel becomes compressed by the prescribed mean amount.

In a separate aspect of the invention, the pressure transducer is in compressive association with the tissue and blood vessel through a substantially incompressible, and preferably compliant plug, whereby the pressure signal is a reasonably accurate representation of the pressure being applied to the plug by the

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tissue. The plug preferably fills a chamber that connects the pressure transducer to the tissue. For the purposes of this application, a plug is broadly defined to be any intermediary device that puts the pressure transducer in compressive association with the tissue. For example, the plug might comprise a liquid sealed into a chamber by a
5 flexible diaphragm, where the diaphragm contacts the tissue and the liquid contacts the pressure transducer. Likewise, the plug might be a rigid, solid device in contact with both the pressure transducer and the tissue.

In another separate aspect of the invention, the pressure transducer is
10 configured to be in compressive association with a first portion of the tissue overlying the subject's blood vessel. A compression surface of the device is configured to compress a second portion of the tissue overlying the subject's blood vessel, the second portion preferably being a section of tissue surrounding the first portion of the tissue. The compression surface preferably compresses the second portion of tissue in concert
15 with the pressure transducer's compressing of the first portion of tissue. This will preferably cause the pressure transducer to only sense the pressure immediately beneath it, minimizing edge effects and the pounding of artery pressure against the edge of the occluded section of the vessel.

20 It is also preferable that the compression surface includes an inner section and an outer section, the outer section being more compliant than the inner section. This may, in some embodiments, further minimize edge effects and pounding, as well as potentially adding to the subject's comfort due to the compliant portion forming a radius to transition between the compressed and non-compressed portions of the arm.

25

Another aspect of the invention resides in a blood vessel sensor carried on a housing that contains the pressure transducer. The blood vessel sensor is configured to detect the presence, and preferably the location, of a blood vessel such as an artery, thus allowing the pressure transducer to be placed in a prescribed position overlying the
30 subject's blood vessel. The blood vessel is preferably a blood flow sensor that senses the

flow (although, not necessarily the flux) of blood in the space adjacent to the housing. The blood flow sensor is preferably an ultrasonic transducer having a substantially planar face that is oriented at a prescribed acute angle relative to a planar face of the housing that adjoins the tissue overlying the blood vessel (e.g., the compression surface).

5 The ultrasonic transducer preferably senses the velocity of the blood flow, providing an indication of blood flow when the velocity is sensed. Preferably there is a coupling medium disposed on the planar face, which in various embodiments can enhance the coupling between the ultrasonic transducer and the subject's blood vessel, and can aid in the positioning of the pressure transducer.

10

In another embodiment, the invention may feature a controller configured to controllably modulate the position of a pressure sensor assembly relative to a nominal location (and the subject's blood vessel) with a periodic signal having a frequency substantially greater than the frequency of the subject's expected heartbeat, and the
15 controller monitors the resulting pressure signal to produce a plurality of pressure waveforms. Each such pressure waveform corresponds to a different phase of the periodic signal, which in turn corresponds to a different nominal amount of vessel compression.

20

The controller is configured to select the particular one of the pressure waveforms that derives from a selected transmural pressure, preferably being a transmural pressure of substantially zero. For example, the waveform may be selected by choosing the particular waveform for which the pressure signal at systole differs from the pressure signal at diastole by a maximum amount. The controller then directs the
25 coupling device to adjust the nominal location such that the selected waveform generally exhibits a lower mean pressure than half of the waveforms and exhibits a higher mean pressure than the other half of the waveforms.

Other features and advantages of the present invention should become
30 apparent from the following description of the preferred embodiments, taken in

conjunction with the accompanying drawings, which illustrate, by way of example, the principles of the invention.

5

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a partial, perspective view of a blood pressure monitoring apparatus embodying features of the present invention. Depicted are a base plate, a coupling device and a pressure sensor assembly of the blood pressure monitoring apparatus.

10

FIG. 2 is a schematic cross-sectional view of the blood pressure monitoring apparatus of FIG. 1, in its prescribed position secured to a subject's wrist, with the pressure sensor assembly disposed adjacently to the tissue overlying the subject's radial artery.

15

FIG. 3 is a view of the base plate, coupling device and pressure sensor assembly of FIG. 1, from a different perspective than that of FIG. 1.

20

FIG. 4 is a perspective view of the base plate, coupling device and pressure sensor assembly of FIG. 1, wherein the coupling apparatus has retracted the pressure sensor assembly.

25

FIG. 5 is a perspective view of the base plate, coupling device and pressure sensor assembly of FIG. 1, wherein the coupling apparatus has advanced the pressure sensor assembly.

30

FIG. 6 is an exploded perspective view of a sensor housing that is part of the pressure sensor assembly of FIG. 1.

FIG. 7 is a cross-sectional view of the sensor housing of FIG. 6.

FIG. 8 is a block diagram of a first embodiment of a blood pressure monitoring apparatus in accordance with the invention, incorporating the coupling
5 device and pressure sensor assembly of FIG. 1.

FIG. 9 is a block diagram of a second embodiment of a blood pressure monitoring apparatus in accordance with the invention, which incorporates the coupling device and pressure sensor assembly of FIG. 1 and provides an accurate depiction of a
10 subject's arterial pressure waveform within as little as a single heartbeat.

FIG. 10A is a graph of an exemplary pressure signal produced by the blood pressure monitoring apparatus of FIG. 9, incorporating both a sinusoidal modulation component and a subject heartbeat component.
15

FIG. 10B is a graph of ten reconstructed pressure waveforms reconstructed from the exemplary pressure signal of FIG. 10A by the blood pressure monitoring apparatus of FIG. 9.

FIG. 11 is a block diagram of the signal processing portion of an ultrasound system, used to controllably position pressure sensor assembly of FIG. 1 on a subject's wrist.
20

25 DESCRIPTION OF THE PREFERRED EMBODIMENTS

Preferred embodiments of the present invention include variations of the apparatus and methods described below. The embodiments incorporate aspects of the invention described in the U.S. Patent entitled "Apparatus and Method for

Non-invasively Monitoring a Subject's Arterial Blood Pressure,"

Patent No. 5,848,970 issued December 15, 1998.

With reference now to the drawings, and particularly to FIGS. 1 and 2,
5 there is shown a blood pressure monitoring apparatus 10 configured for attachment to a subject's wrist 12, with a pressure sensor assembly 14 compressively engaging the tissue 16 overlying the subject's radial artery 18. Blood pressure variations within the artery are coupled through the tissue to the pressure sensor assembly, to produce a pressure signal output that represents the artery's pressure waveform. The pressure sensor
10 assembly, by engaging the tissue over the radial artery, compresses the radial artery, generally causing a partial or total occlusion of the vessel. The amount of compression affects the degree of coupling between the pressure variations within the artery and the pressure applied to the pressure sensor assembly.

15 As seen in FIGS. 1 - 3, the blood pressure monitoring apparatus 10 includes a plastic plate-like base 20 having a curved shape to conform to the subject's wrist 12. The base defines an orifice 22 configured such that the pressure sensor assembly 14 can advance through the orifice to contact the tissue 16 overlying the subject's radial artery 18. A snap-fit type / quick-release attachment 24 is formed on the
20 base, allowing the base to quickly and easily receive a coupling device 26 configured to control the advancement of the pressure sensor assembly through the orifice, and thus to control the location of the pressure sensor assembly.

The base 20 also includes attachment loops 28 configured to receive a
25 wrist strap 30 to hold the base in a prescribed position on the subject's wrist 12. When the blood pressure monitoring apparatus 10 is properly secured to the subject's wrist, it holds and maintains the pressure sensor assembly 14 in a location appropriate to advance into contact with the tissue 16 overlying the subject's radial artery 18.

The coupling device 26 includes a first electric motor 32, a second electric motor 34, and a lever arm 36. The two motors are affixed to a coupling device attachment (not shown) conforming to the snap-fit attachment 24 on the base 20. Thus, when the coupling device attachment is received in the base's attachment, the two
5 motors are held in a substantially fixed position with respect to the base. Preferably, the motors' axes are at right angles to the surface of the tissue 16 overlying the subjects radial artery 18, and most preferably the motors' axes are approximately parallel to the artery.

10 The lever arm 36 is suspended between a first, eccentrically located cam 38 on the first motor 32, and a second, eccentrically located cam 40 on the second motor 34. Each cam 38, 40 is received within a respective slot 42, 44 on opposing ends of the lever arm, allowing the motors to drive the cams and thereby exercise control over the lever arm's orientation and location. The pressure sensor assembly 14 is connected to a
15 central portion of the lever arm, between the two slots, by a pin 46. The motors and lever arm are thus configured such that either motor may affect the location of the pressure sensor assembly.

The first cam 38 is attached to the first motor 32 with a relatively large
20 amount of eccentricity, relative to the second cam and motor, thus providing for relatively large controlled movements of the pressure sensor assembly 14. This can be seen in FIGS. 4 and 5, showing the pressure sensor assembly 14 retracted and advanced, respectively, by the first motor 32 and the first cam 38. The second cam 40 is attached to the second motor 34 with a relatively small amount of eccentricity, providing for
25 comparatively smaller controlled movements of the pressure sensor assembly, which are not depicted.

While the motors 32, 34, their respective eccentric cams 38, 40, and the lever arm 36 provide for a preferred form of coupling device 26, a wide variety of

variable positioning devices, or combinations of variable positioning devices, would be suitable for use with the invention.

With reference to FIGS. 1, 6 and 7, the pressure sensor assembly 14 includes a sensor frame 48, a sensor housing 50, and a pressure transducer 52. The sensor frame is hingedly attached to the lever arm 36 by the pin 46, and thus can pistonicly convert translational and rotational movement of the lever arm, caused by the cams, into a translational motion. The sensor housing includes two flanges 54 (see FIG. 5) that conform to two slots in the sensor frame, providing for the sensor housing to be slidably removable from the sensor frame for ease of service and replacement. The pressure transducer is carried by the sensor housing, and is configured to convert pressure applied against it to an electrical signal indicative of the pressure level.

The sensor housing includes a substantially rigid, preferably plastic portion 56 that includes the flanges 54, and also includes a protrusion 58 having a roughly oval / elliptical cross-section (i.e., having a cross-sectional length greater than a cross-sectional width, and having rounded corners). The cross-sectional length is preferably configured to extend along the blood vessel, thus providing compression along a length of vessel while minimizing the compression of surrounding tissue, and minimizing interference from bones and tendons. Alternatively, the rigid portion may be metal or some other relatively rigid material. It may be preferable that the rigid portion is more compliant than bone, and is less compliant than interstitial tissue and arterial wall.

The protrusion is surrounded by a conforming ring 60 composed of a relatively compliant material such as room temperature vulcanizing rubber (RTV) or silicone. The protrusion and the ring include surfaces combining to form a flat compression surface 62 that is relatively rigid in an inner section (the protrusion) and relatively compliant in an outer section (the ring).

30

The compression surface 62 is interrupted by an opening to a chamber 64, formed in the protrusion 58. The chamber extends from the compression surface up to the pressure transducer 52. The chamber is preferably filled with a plug 66, in the form of an incompressible, and preferably compliant material, such as RTV. The plug forms a surface, across the chamber opening, that is flush with the compression surface. Filling the chamber entirely, the plug also presses up against the pressure transducer. Thus, when the sensor housing 50 is pressed against the tissue 16 overlying the subject's radial artery 18, the pressure transducer is in compressive association, through the plug and the skin directly underlying the plug, with a first portion of the tissue overlying the subject's radial artery, and thus with the radial artery itself.

At the same time, the compression surface 62 compresses a second portion of the tissue overlying the subject's radial artery 18, the second portion of the tissue surrounding the first portion of the tissue. The sensor housing, the pressure transducer and the plug all move in conjunction with each other, providing for the first and second portions of the tissue to be compressed in a flush, uniform fashion. This provides for the portion of the artery that is compressed and occluded to extend beyond the more limited portion that is in compressive association with the pressure transducer 52, and thus shields the pressure transducer from spurious pressure information caused by the blood in the artery having to pass into the portion of the artery that is compressed and occluded. It also diminishes the flow to the artery underlying the pressure sensor during periods of positive transmural pressure.

As is described in the U.S. Patent 5,848,970, if the artery 18 is compressed by an amount that corresponds to a mean transmural pressure near zero, the pressure variation of a normal heartbeat, about 50 mmHg (i.e., 50 millimeters of mercury) will cause a relatively large change in the artery's effective diameter, as compared to the artery's change in diameter at non-zero mean transmural pressures. This provides for a maximum coupling between the arterial pressure and the pressure transducer's output

signal. It is desirable, therefore, to regulate the mean arterial compression to match this optimum value.

To this end, the coupling device 26 controls the location of the pressure
5 sensor assembly 14. In particular, the coupling device implements a control scheme that
locates the pressure sensor assembly so as to compress the tissue 16 overlying the
subject's radial artery 18 to provide optimal compression of the radial artery. While a
preferred control scheme is to maintain the mean transmural pressure at zero, a variety
of other requirements (e.g., holding either the mean pressure or the maximum and
10 minimum pressures within prescribed bounds) might alternatively be prescribed to
produce optimal or preferable results.

Under the preferred control scheme, the coupling device 26 actively
varies, or modulates, the location of the entire pressure sensor assembly 14, including
15 the pressure transducer 52, toward and away from the blood vessel, relative to a nominal
location. For example, the coupling device could sinusoidally cycle the pressure sensor
assembly relative to a nominal location that is the mean position of the cycle. The
modulating location of the pressure sensor assembly modulates, or dithers, the
compression of, and thereby the effective diameter of, the subject's radial artery 18
20 underlying the pressure sensor assembly. The effect of the modulating artery diameter
on the pressure signal is then analyzed, providing information on the transmural
pressure, as is described in the U.S. Patent 5,848,970.

The coupling device 26 effects this modulation of the artery's diameter by
25 imparting a 25-Hz sinusoidal motion to the pressure sensor assembly 14. This
sinusoidal motion is produced by the second motor rotating at 25-Hz, causing the second
cam to move one end of the lever arm at that rate. A 25-Hz frequency is selected,
because it is generally higher than the highest frequency components of interest in the
artery's blood pressure waveform, and thus the pressure signal may be accurately filtered
30 for its modulation and heartbeat components.

If the artery 18 is under-compressed, then the ac pressure response to the 25-Hz oscillation will be larger during systole than during diastole. Conversely, if the artery is over compressed, then the ac amplitude of the 25-Hz pressure oscillation will be larger during diastole than during systole. However, if the artery 21 is optimally
5 compressed, then the ac amplitudes of the 25-Hz pressure oscillation during the systolic and end-diastolic stages will be substantially the same. In addition, the overall amplitude of the pressure oscillation is at a minimum when the artery is optimally compressed. With this information, regarding the under- or over-compression of the artery, the movement of the pressure sensor assembly 14 may be adjusted such that the
10 nominal location moves toward a target location at which the artery is compressed to the optimum mean amount.

A control system for implementing the control scheme described above is depicted in FIG. 8. An oscillator 100 controls the speed of the second motor 34 to
15 cyclically compress the artery 18 at 25-Hz. In addition to the coupling device 26 and the pressure sensor assembly 14, identified above, the control system further includes a 25-Hz bandpass filter 102 that filters the pressure signal received on line 104 from the pressure transducer 52.

20 The filtered signal, which incorporates only the 25-Hz component of the pressure signal, is supplied on line 106 to an analyzer 108. The analyzer receives the filtered signal and compares its ac amplitude during systole with its ac amplitude during diastole, to determine whether the artery is under compressed, over compressed, or optimally compressed. The analyzer then produces a corresponding error signal that is
25 supplied on line 110 to the first motor 32, which adjusts the lever arm 36 to appropriately adjust the nominal location toward the target location.

Operation of the controller system automatically regulates the position of the pressure sensor assembly 14 such that the assembly optimally compresses the
30 subject's radial artery 18. For example, if the analyzer 108 determines that the ac

amplitude of the filtered pressure signal is greater during systole than it is during diastole, then a positive error signal is produced, and the first motor 32 is adjusted to advance the nominal location of the pressure sensor assembly and thereby increase the compression of the artery. The opposite would occur if the controller determines that
5 the filtered pressure signal's ac amplitude is greater during diastole than it is during systole.

To provide a visible display of the subject's arterial pressure waveform, the blood pressure monitoring apparatus 10 further includes a 25-Hz band stop filter 112
10 and a display 114. The filter receives the pressure signal on line 104 from the pressure transducer 52, and it samples this signal at a rate of 50 samples per second. This sampling is phased with the 25-Hz modulation signal output on line 116 by the oscillator 100 such that it always occurs at the modulation signal's zero crossings. The sampled pressure signal then is coupled on line 118 to the display 120, for real-time display. The
15 sampled pressure signal is also coupled on line 118 to the analyzer 108, to be used for determining the timing of systole and diastole.

In an independent feature of the invention, an accurate depiction of the subject's blood pressure waveform, and an accurate measurement of arterial pulse
20 pressure amplitude, can be produced within as little as a single heartbeat using a monitoring apparatus embodying the invention under a control system, as depicted in FIG. 9, which implements a special control and monitoring algorithm. Some elements of the apparatus of FIG. 9 correspond to elements of the apparatus of FIG. 8, and these elements are identified by the same reference numerals, but with an added prime (')
25 symbol.

More particularly, and with reference to FIG. 9, coupling device 26', including a first motor 32', a second motor 34', and a lever arm 36', are configured to advance a pressure sensor assembly 14' against the tissue overlying the radial artery 18.
30 The pressure sensor assembly includes a pressure transducer 52' that is configured to be

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held in compressive engagement with the tissue by a wrist strap. Actually, because the pressure waveform ordinarily can be produced within merely a few seconds using this feature, the wrist strap can be eliminated and the apparatus operated simply by pressing the device manually against the subject's wrist.

5

An oscillator, or timing circuit 100' supplies a 25-Hz sine wave signal on line 116' to the second motor 34', to cause the pressure sensor assembly 14' to be modulated, i.e., advanced into and retracted from the tissue overlying the artery 18, in a sinusoidal fashion, with respect to a nominal location. If the pressure sensor assembly is
10 being urged against the subject's wrist such that the arterial wall is partially compressed, this modulation ordinarily will cause a corresponding sinusoidal pressure variation about a mean pressure on the pressure transducer 52'. The pressure transducer replicates this pressure variation in an analog pressure signal output on line 104'.

15

One representative waveform for the analog pressure signal on line 104' is depicted in FIG. 10A, which corresponds to a situation in which the pressure sensor assembly 14' is being urged against the subject's wrist with a mean pressure of about 80 mmHg. It will be noted that the pressure signal includes not only a 25-Hz modulation component, but also a heartbeat component. The apparatus of FIG. 9 functions
20 effectively to demodulate this waveform and thereby to produce an accurate representation of the subject's actual blood pressure waveform.

25

The apparatus of FIG. 9 achieves this demodulation by sampling the analog pressure signal on line 104' at a sample rate that is an integral multiple of the 25-Hz modulation frequency. At a sample rate of 1600-Hz, for example, 64 samples would be provided for each modulation cycle. Since the first sample of each successive modulation cycle is produced while the 25-Hz modulation component is at the same level, it follows that these first samples can be associated together to produce a depiction of the subject's variable arterial pressure for that particular level. The same is true for

each of 64 separate sets of samples. Thus, 64 separate pressure waveforms can be generated, each representing a different nominal arterial compression.

Ten exemplary waveforms of these 64 separate pressure waveforms are depicted in FIG. 10B. It will be noted that the waveform having the lowest magnitude represents the pressure samples that are made when the 25-Hz modulation waveform is at its lowest value, and that the waveform having the highest magnitude represents the pressure samples that are made when the 25-Hz modulation waveform is at its highest value. The particular one of the waveforms that provides the greatest difference between the systolic pressure and diastolic pressure is deemed to be the one produced when the subject's artery is compressed by the particular amount that provides optimal coupling to the pressure transducer 52'. In the exemplary case depicted in FIG. 10B, this particular waveform is depicted by the bold reference line G.

It will be appreciated that the particular one of the 64 waveforms that is considered optimal will vary depending on the nominal pressure applied by the pressure sensor assembly 14' to the subject's wrist. If the nominal pressure is relatively low, then the optimal waveform will likely be one of the higher-level waveforms, which are produced when the 25-Hz modulation signal is at or near its positive peak. On the other hand, if the nominal pressure is relatively high, then the optimal waveform will likely be one of the lower-level waveforms, which are produced when the 25-Hz modulation signal is at or near its negative peak.

With reference again to FIG. 9, the successive samples of the analog pressure signal on line 104' are produced by a sample-and-hold or sampler circuit 150, under the guidance of a 1600-Hz clock signal supplied on line 152 from the timing circuit 100'. The resulting samples are supplied on line 154 to an analog-to-digital converter 156, which produces a succession of digital words that are coupled on lines 158 to a suitable processor 160. The processor associates together the successive samples, as discussed above, acting as a comb filter to produce the 64 separate

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waveforms. It then ascertains the particular waveform that corresponds to the optimum level of nominal artery compression, which is preferably the waveform having the largest pulse amplitude. This particular waveform is then coupled via line 162 to a display 120'.

5

While the optimal waveform may be any of the 64 waveforms, it is preferable that the optimal waveform is close to or exactly the middle waveform. This provides for the artery to have a mean transmural pressure of approximately zero throughout the modulation. To close the loop, providing feedback to appropriately adjust the nominal pressure, the processor 160 analyses the relative levels of the optimal waveform with respect to the other waveforms. Preferably, the processor compares the arithmetical average (i.e., mean) pressure for each set of waveform data. If the optimal waveform is at a lower pressure than most waveforms, then the nominal pressure applied to the wrist should be reduced. Similarly, if the optimal waveform is at a higher pressure than most, then the nominal pressure applied to the wrist should be increased.

After each heart beat, the processor determines the desired change to the nominal pressure, if any, and provides this information on line 164 to a control logic circuit 166 that controls the first motor 32'. The first motor then actuates the lever arm 36' to adjust the nominal location of the oscillation toward a target location where the pressure sensor assembly 14' compresses the artery 18 to have a mean transmural pressure of approximately zero. As the optimal waveform approaches the middle of the waveforms, the amplitude of the 25-Hz modulation may be reduced to maintain the high and low transmural pressures near the mean transmural pressure at approximately zero.

25

The apparatus of FIG. 9 can be used with sampling rates of varying multiples of the modulation frequency, with higher rates being preferable for accuracy, and lower rates being preferable for computational simplicity. Furthermore, numerical approximation techniques can be used to practice this invention without having a

sampling frequency that is a precise multiple of the modulation rate, however, such an embodiment is not preferred.

The two embodiments described above, incorporating the two distinct
5 features of the invention, being depicted in FIGS. 8 and 9, both presume that the pressure sensor assembly 14 or 14' is correctly circumferentially positioned with respect to the arm in order to properly compress the artery 18. While skilled professionals and/or experienced subjects might become proficient at placement of the blood pressure monitoring apparatus 10, the device preferably includes a mechanism designed to guide
10 the circumferential positioning of the pressure sensor assembly with respect to the subject's arm.

To this end, with reference to FIG. 7, the blood pressure monitoring apparatus 10 further incorporates a blood vessel sensor, preferably in the form of a
15 blood flow sensor. The blood flow sensor could be of any functional type, such as using lamps, tones, or the like, and could sense any type of characteristic indicative of blood flow, such as blood velocity. The blood flow sensor is preferably an ultrasound system for use in controllably positioning the pressure sensor assembly 14 in its prescribed position immediately overlying the subject's radial artery 18. Other sensors capable of
20 detecting the presence of a blood vessel (including those capable of detecting the presence of blood) are within the scope of the invention.

The ultrasound system includes an ultrasonic transducer 200 in the form of a piezoelectric device, which is carried within a recess 202 of the plastic portion 56 of
25 the sensor housing 50, adjacent to the chamber 64 that carries the pressure transducer 52. The ultrasonic transducer is conditioned to emit a series of ultrasonic bursts into the tissue adjacent to the pressure transducer.

The bursts are scattered by red blood cells flowing through the artery, and
30 the ultrasonic transducer receives back a portion of the scattered bursts. The scattered

bursts are Doppler shifted according to the velocity of the blood. The ultrasound system then compares the frequencies and phase angles of the transmitted and returned bursts, and it monitors the magnitude of the comparison signal to determine the proximity of the ultrasonic transducer to the artery. This allows the pressure sensor assembly to be
5 controllably moved across the subject's wrist until its prescribed position overlying the radial artery has been reached. Optionally, this may also be used to determine the blood flow velocity.

More particularly, the oval shape of the compression surface conveniently
10 allows for the pressure transducer and the ultrasonic transducer to be conveniently placed next to each other. The sensor housing recess 202 that carries the ultrasonic transducer 200 has a shape that is generally oriented at an angle of about 35 degrees relative to the sensor housing's planar compression surface 62, facing the pressure
15 transducer chamber 64. The ultrasonic transducer is secured within its recess, and it is conditioned to emit bursts of ultrasonic energy axially out of the recess, into the space immediately underlying the pressure transducer chamber. With the oval shape aligned with the vessel, the ultrasonic transducer may be positioned downstream (relative to the blood flow) from the pressure transducer, emitting the bursts in an upstream direction. In order to improve the connection between sensor housing and the skin, air gaps are
20 preferably removed using some form of gel. Alternatively, a semi-cured, sticky (tacky) RTV could be used.

Because of the specified acute angle, a component of the emitted bursts inherently will be aligned with the axis of the subject's radial artery 18, such that the
25 flow of blood through the artery can be readily detected using standard Doppler detection. An ultrasonic transducer 200 orientation angle in the range of about 30 to 60 degrees is considered suitable, although 35 degrees is preferred. Upon passing through the material interface from the sensor housing to the tissue, waves from the ultrasonic transducer bend to a preferred angle of 45 degrees.

30

FIG. 11 is a simplified block diagram of the signal processing portion of the ultrasound system, used to controllably position the pressure sensor assembly 14 in its prescribed position on the subject's wrist. An oscillator 204 generates a continuous square wave signal, having a fixed frequency of about 8 MHz, for coupling to a gate logic circuit 206 and to an rf mixer 208. The gate logic circuit transmits 8 microsecond bursts of the 8 MHz signal, interrupted by 8 microsecond dead times. An rf shaper circuit 210 converts the resulting series of square wave bursts from the gate logic circuit into corresponding sine wave bursts, for application to the ultrasonic transducer 200. The ultrasonic transducer thereby is conditioned to transmit a succession of 8 MHz bursts of sonic energy into the adjacent tissue.

In use, the transmitted bursts of sonic energy are scattered by red blood cells flowing through the subject's radial artery 18, and a portion of the scattered energy is directed back toward the ultrasonic transducer 200. The time required for the return energy to reach the ultrasonic transducer varies according to the speed of sound in the tissue and according to the depth of the artery. Typical transit times are in the range of 6 to 7 microseconds.

The ultrasonic transducer 200 is used to receive the reflected ultrasound energy during the dead times between the successive transmitted bursts. The ultrasonic transducer therefore produces a receive signal, of relatively low magnitude, and this receive signal is coupled to an rf amplifier 212, for amplification. The amplified signal is then supplied to an rf switch 214, which gates the signal to the rf mixer 208 only during the dead times between successive transmitted bursts. The rf mixer mixes these gated bursts with the original 8 MHz signal received from the oscillator 204.

The frequency of the ultrasonic transducer's transmit signal will differ from that of the return signal, because the scattering red blood cells within the radial artery 18 are moving. Thus, the return signal, effectively, is frequency modulated by the blood flow velocity. The signal output by the rf mixer 208, therefore, will incorporate

the 8 MHz fundamental frequency, as well as sum and difference frequencies of the transmit and return signals. This output signal is supplied to a low-pass filter 216, for removal of the 8 MHz fundamental frequency, as well as any higher-order harmonics. A bandpass filter 218 then removes all signal components other than those components
5 representing the actual blood velocity.

The signal output by the bandpass filter 218 is supplied to an audio amplifier 220, and in turn to a speaker 222, to enable an operator to hear a representation of the blood velocity signal and thereby to determine when the pressure
10 sensor assembly 14 is located approximately over the radial artery 18. The output signal also is supplied to a zero-axis crossing detector 224, which functions like a one-shot circuit to produce a pulse each time the signal crosses a zero axis. These pulses are supplied to a frequency-to-voltage converter circuit 226, which produces a dc output signal indicative of frequency and thus of the blood flow rate. This signal can be
15 displayed and/or recorded for further analysis.

In an alternative embodiment (not shown in the drawings), the ultrasound system includes an array containing a plurality of ultrasonic transducers, preferably being three or more transducers, arranged along an axis perpendicular to the direction
20 toward the pressure transducer 52. By comparing the relative strengths of the signals derived from the ultrasonic transducers, a determination of the correct direction for moving the pressure sensor assembly 14 to its prescribed position overlying the subject's radial artery 18 can be readily ascertained. A lateral adjustment mechanism, such as a turn screw, may be manually driven in response to the error signal, or may be
25 automatically controlled by a controller in response to the error signal.

In another alternative embodiment (likewise not shown in the drawings), a single ultrasonic transducer is configured to be controllably tiltable, so as to sweep its ultrasound bursts across the subject's wrist. The particular tilt direction that yields a
30 Doppler signal of maximum strength indicates how the pressure sensor assembly 14

must be moved to reach its prescribed position overlying the subject's radial artery 18. This system preferably provides directional information for the position of the blood vessel. Alternatively, the transducer tilting mechanism can be replaced by a reflector with a tilting or turning mechanism that oscillates to steer the signals.

5

Various embodiments of the invention may provide for displays that include information on the systole, the mean, the diastole, the heart rate, the time-tension index and the pressure waveform. The information may be graphically and/or numerically presented. Furthermore, the information may be passed to data storage machines or other devices requiring the information.

10

It should be appreciated from the foregoing description that the present invention provides an improved apparatus for monitoring a subject's blood pressure, non-invasively, in which a pressure sensor assembly, incorporating a pressure transducer, is compressed against tissue overlying an artery with sufficient force to compress the artery by an amount that optimally couples pressure waveforms within the artery. In addition, while the position of the pressure sensor assembly is modulating, the nominal location of the pressure sensor assembly is controlled to compensate for pressure variations due to arterial pulses. This minimizes variations in the artery's effective diameter, whereby the pressure applied to the pressure transducer is made to closely follow the actual arterial pulse waveform.

15

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Although the invention has been described in detail with reference only to the preferred embodiments, those skilled in the art will appreciate that various modifications can be made without departing from the invention. Accordingly, the invention is defined only by the following claims.

WHAT IS CLAIMED:

1. An apparatus for monitoring the pressure within a subject's blood vessel,
 5 comprising:

a housing;

a pressure transducer carried on the housing and producing a pressure signal
 indicative of the pressure applied against it;

a coupling device configured to urge the housing into compressive engagement with
 10 tissue overlying a subject's blood vessel, to compress the vessel such that pressure
 variations within the vessel are coupled through the tissue to the pressure transducer;
 wherein the coupling device comprises a variable positioning device comprising a
 mechanism to modulate the location of the pressure transducer about a nominal location;
 and

15 a controller which controls the variable positioning device so as to perform said
 modulation of the location of the pressure transducer in response to a signal.

2. The apparatus of claim 1, wherein the housing further includes a chamber sized to
 receive the pressure transducer and a recess sized to receive a blood vessel sensing device.

3. The apparatus of claim 1, further comprising a lever arm connected to the
 20 housing, and a second variable positioning device configured to controllably adjust a
 nominal location of the pressure transducer by actuating a first portion of the lever arm.

4. The apparatus of claim 1, wherein the coupling device includes a wrist strap
 configured to secure the housing to the subject's wrist.

5. The apparatus of claim 3, wherein the variable positioning device includes a
 25 motor configured to rotate an eccentric cam within a slot in the lever arm; and wherein the
 second variable positioning device includes a motor configured to rotate an eccentric cam
 within a slot in the lever arm.

6. The apparatus of claim 1, wherein the controller monitors the effect of the
 pressure transducer's modulation on the pressure signal.

30 7. The apparatus of claim 1, wherein the controller is configured to produce an error
 signal indicative of adjustments to the pressure transducer's position which will cause the
 blood vessel to be compressed according to a prescribed requirement.

8. The apparatus of claim 3, wherein the controller is configured to controllably
 vary the second variable positioning device according to error signal to controllably

position the pressure transducer to cause the subject's blood vessel to be compressed according to a prescribed requirement.

9. The apparatus of claim 7, wherein the error signal is indicative of the deviation of the nominal location from a target location at which the vessel is compressed by a mean
5 amount that provides for a transmural pressure of zero.

10. The apparatus of claim 1 comprising a blood vessel sensing device carried on the housing and configured to detect the presence of the blood vessel in a space adjacent to the housing.

11. The apparatus of claim 10, wherein the sensing device is an ultrasonic
10 transducer having a substantially planar face that is oriented at a prescribed acute angle relative to a planar face of the housing.

12. The apparatus of claim 10, wherein the sensing device is an array of blood vessel sensors, the array of blood vessel sensors being configured to determine a direction to move the pressure transducer to reach a prescribed position overlying the subject's blood
15 vessel.

13. The apparatus of claim 1 further comprising: a sampler configured to periodically sample the pressure transducer's pressure signal; a processor configured to process the sampled pressure signal to produce a plurality of pressure waveforms, each waveform representing the blood vessel pressure at a compression level associated with a
20 specific transmural pressure.

14. The apparatus of claim 13, wherein the sampler samples the pressure transducer's pressure signal at a frequency that is a multiple of a frequency that is characteristic of the pressure transducer's modulation.

15. The apparatus of claim 13, wherein the processor is further configured: to select
25 one of the plurality of pressure waveforms; and to rank the selected waveform relative to the waveforms that were not selected, thereby providing for the controller to produce an error signal indicative of the deviation of the nominal location from a target.

16. An apparatus for monitoring the pressure within a subject's blood vessel, comprising:

30 a housing having an associated pressure transducer that produces a pressure signal relating to the pressure applied against it;

a coupling device that urges the housing into compressive engagement with tissue overlying a subject's blood vessel, to compress the vessel such that pressure variations within the vessel are coupled through the tissue to the pressure transducer;

wherein the coupling device comprises a mechanism for modulating the position of the pressure transducer around a nominal position substantially at a predetermined frequency; and

5 a controller which controls the mechanism for modulating so as to perform said modulation of the position of the pressure transducer in response to a signal applied by said controller.

17. The apparatus of claim 16, further comprising a lever arm connected to the housing, and a variable positioning device configured to controllably adjust the nominal location of the pressure transducer by actuating a first portion of the lever arm.

10 18. The apparatus of claim 16, wherein the coupling device includes a wrist strap configured to secure the housing to the subject's wrist.

19. The apparatus of claim 17, wherein the variable positioning device includes a motor configured to rotate an eccentric cam within a slot in the lever arm.

15 20. The apparatus of claim 16, wherein said predetermined frequency comprises 25 Hz.

21. The apparatus of claim 16, wherein the controller monitors the effect of the pressure transducer's modulation on the pressure signal.

20 22. The apparatus of claim 16, wherein the controller is configured to produce an error signal indicative of adjustments to the pressure transducer's position which will cause the blood vessel to be compressed according to a prescribed requirement.

23. The apparatus of claim 17, wherein the controller is configured to controllably vary the variable positioning device according to an error signal to controllably position the pressure transducer to cause the subject's blood vessel to be compressed according to a prescribed requirement.

25 24. The apparatus of claim 1, comprising a blood vessel sensing device carried on the housing and configured to detect the presence of the blood vessel in a space adjacent to the housing.

30 25. The apparatus of claim 24, wherein the sensing device is an ultrasonic transducer having a substantially planar face that is oriented at a prescribed acute angle relative to a planar face of the housing.

26. The apparatus of claim 24, wherein the sensing device is an array of blood vessel sensors, the array of blood vessel sensors being configured to determine a direction to move the pressure transducer to reach a prescribed position overlying the subject's blood vessel.

27. The apparatus of claim 16, further comprising: a sampler configured to periodically sample the pressure transducer's pressure signal; a processor configured to process the sampled pressure signal to produce a plurality of pressure waveforms, each waveform representing the blood vessel pressure at a compression level associated with a specific transmural pressure.

28. The apparatus of claim 27, wherein the sampler samples the pressure transducer's pressure signal at a frequency that is a multiple of a frequency that is characteristic of the pressure transducer's modulation.

29. The apparatus of claim 27, wherein the processor is further configured: to select one of the plurality of pressure waveforms; and to rank the selected waveform relative to the waveforms that were not selected, thereby providing for the controller to produce an error signal indicative of the deviation of the nominal location from a target.

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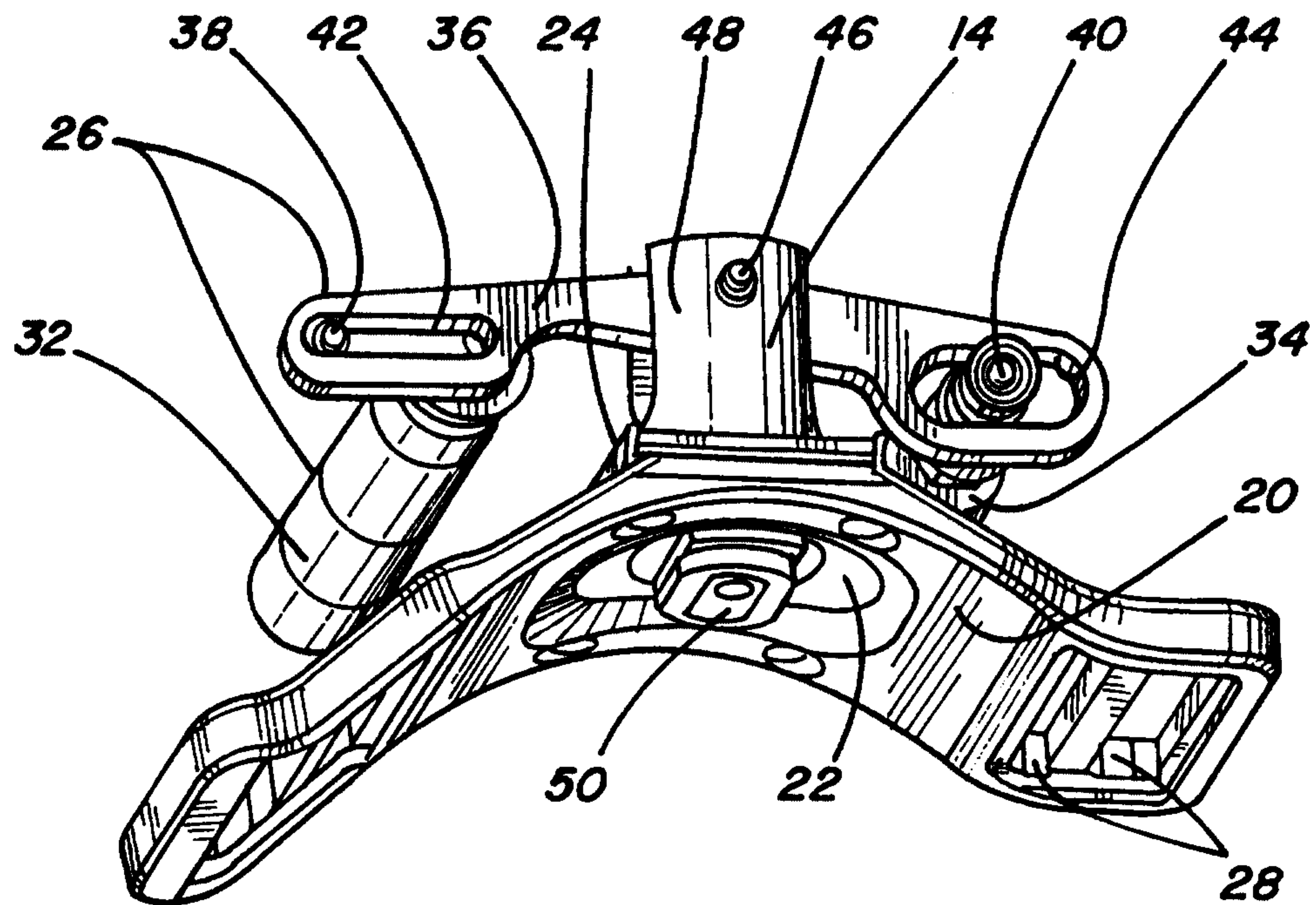


FIG. 1

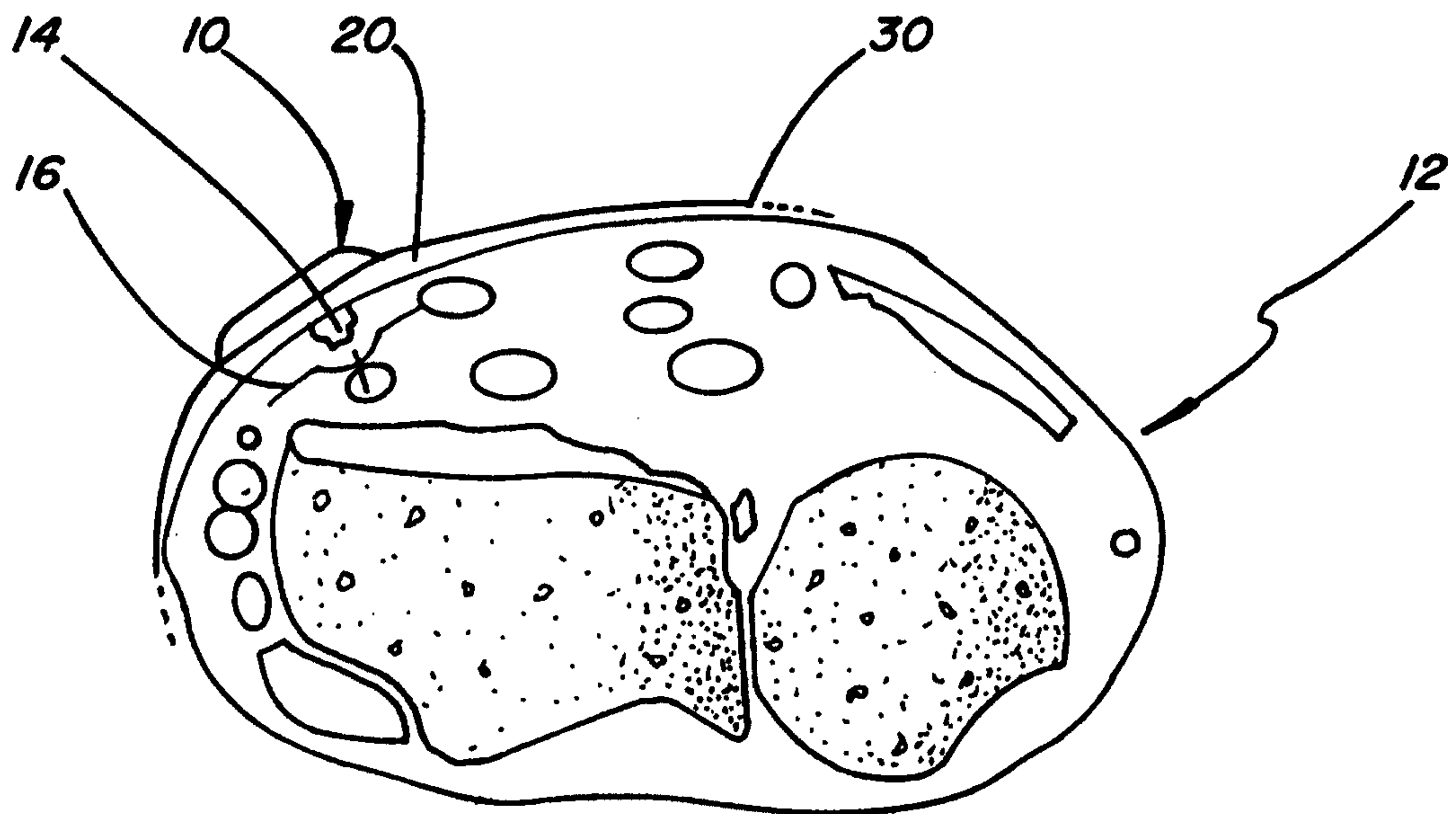


FIG. 2

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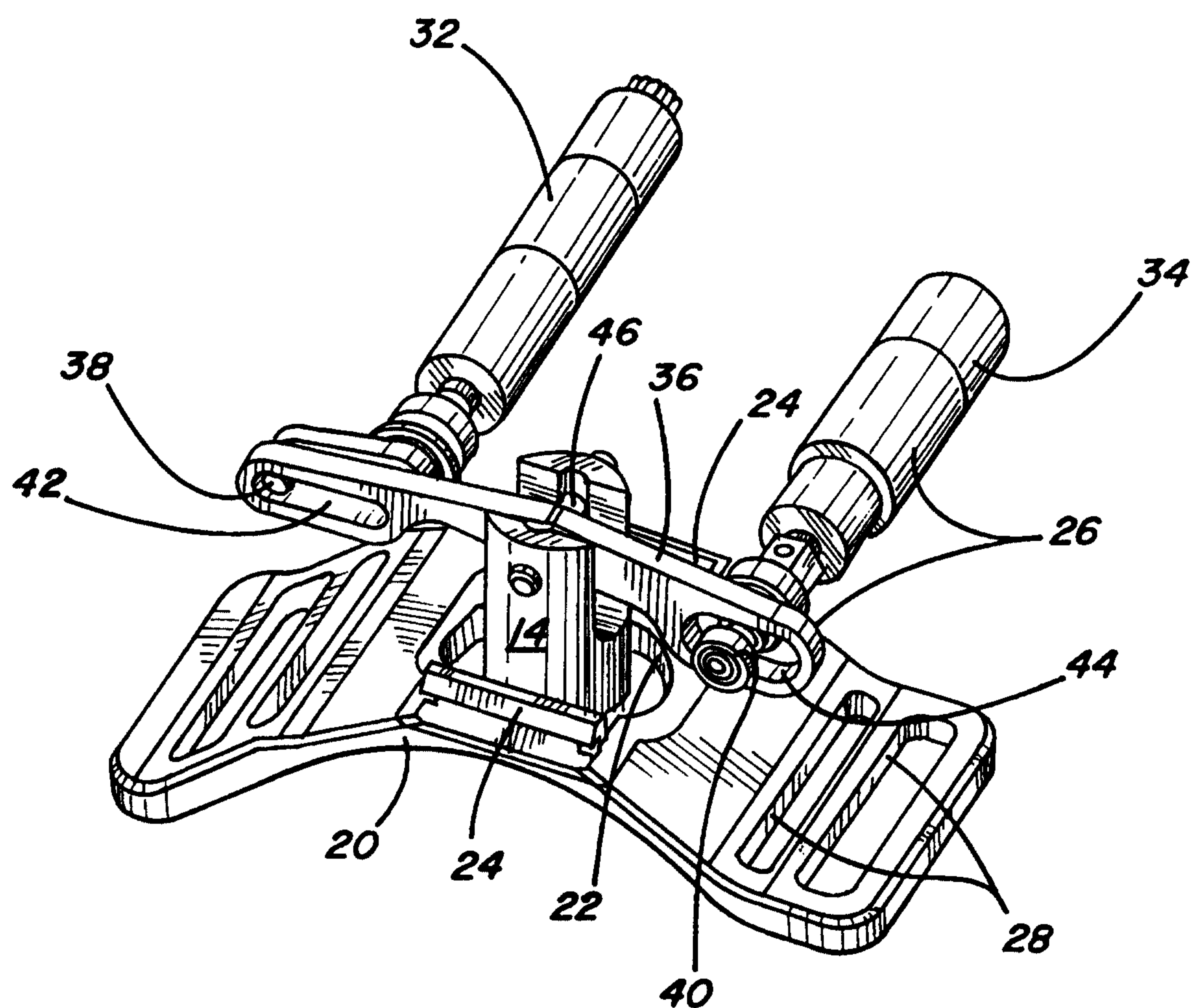
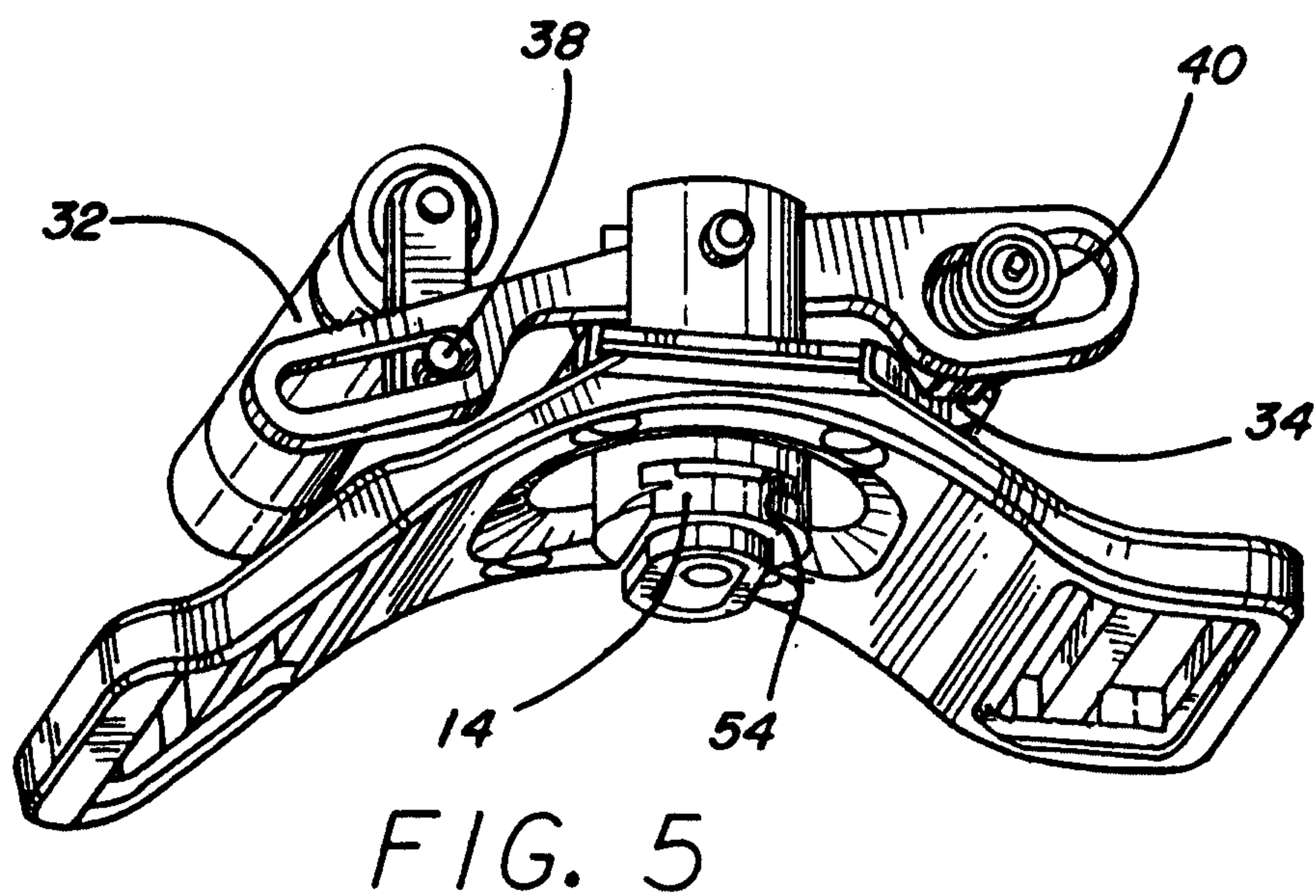
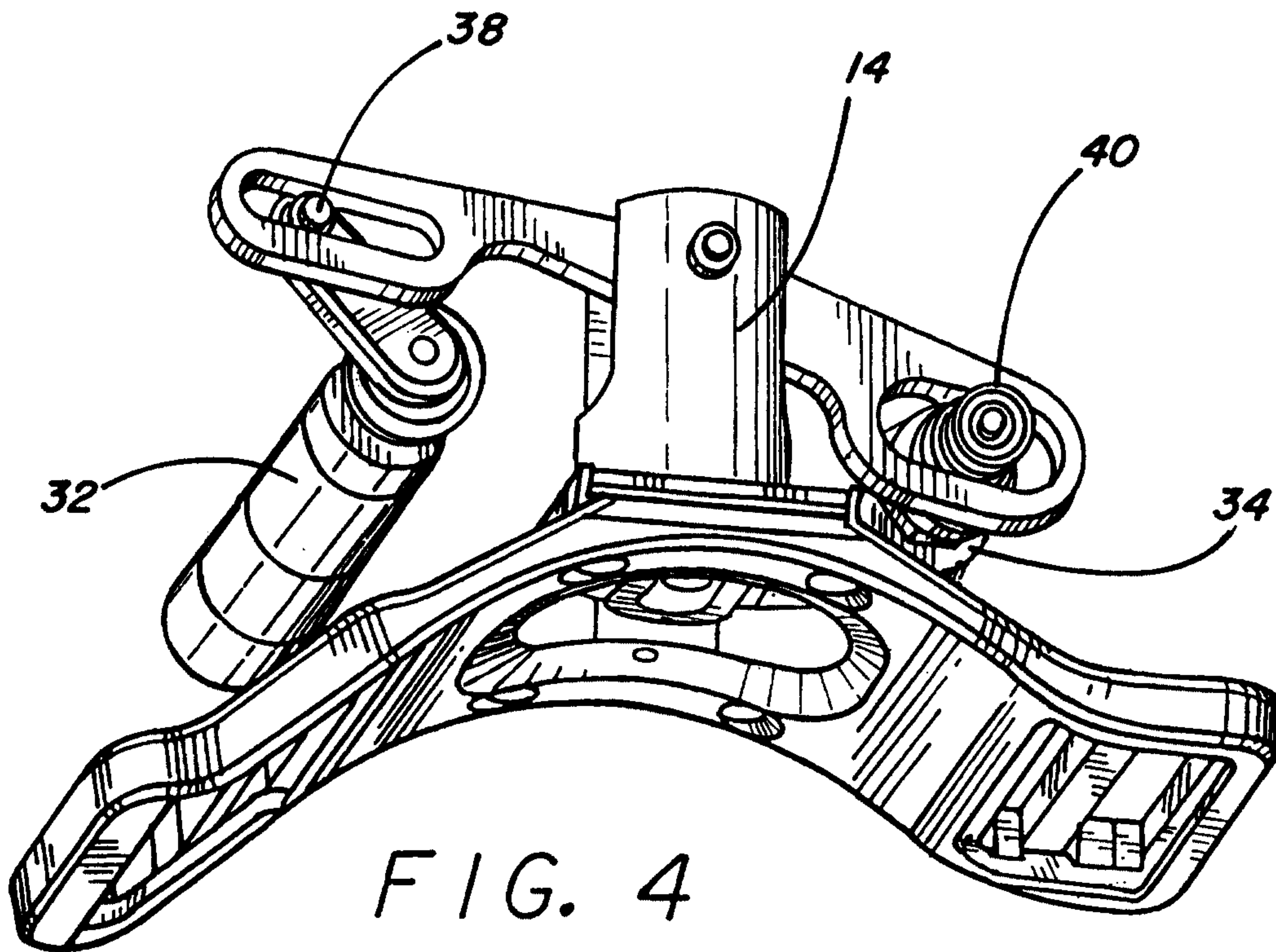
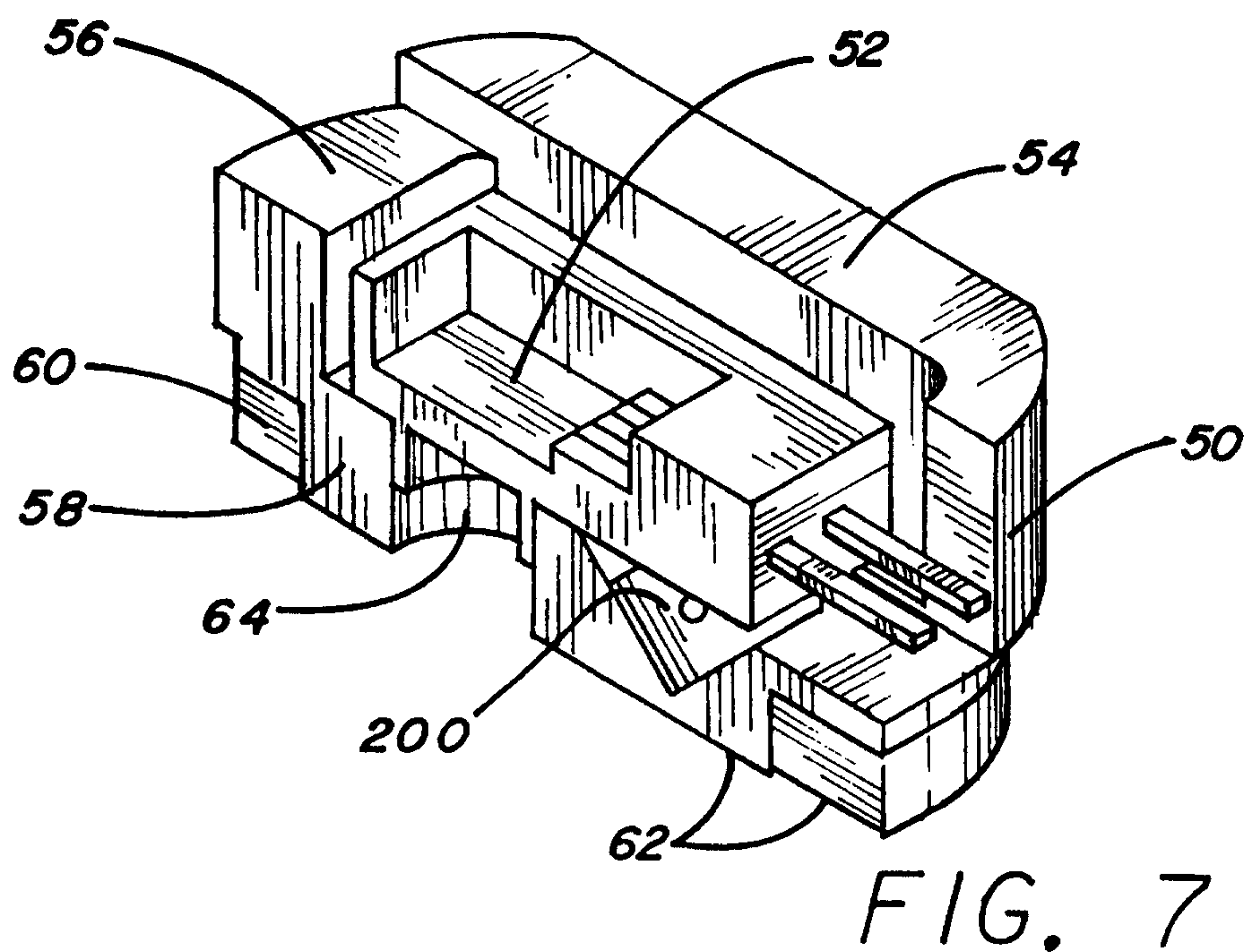
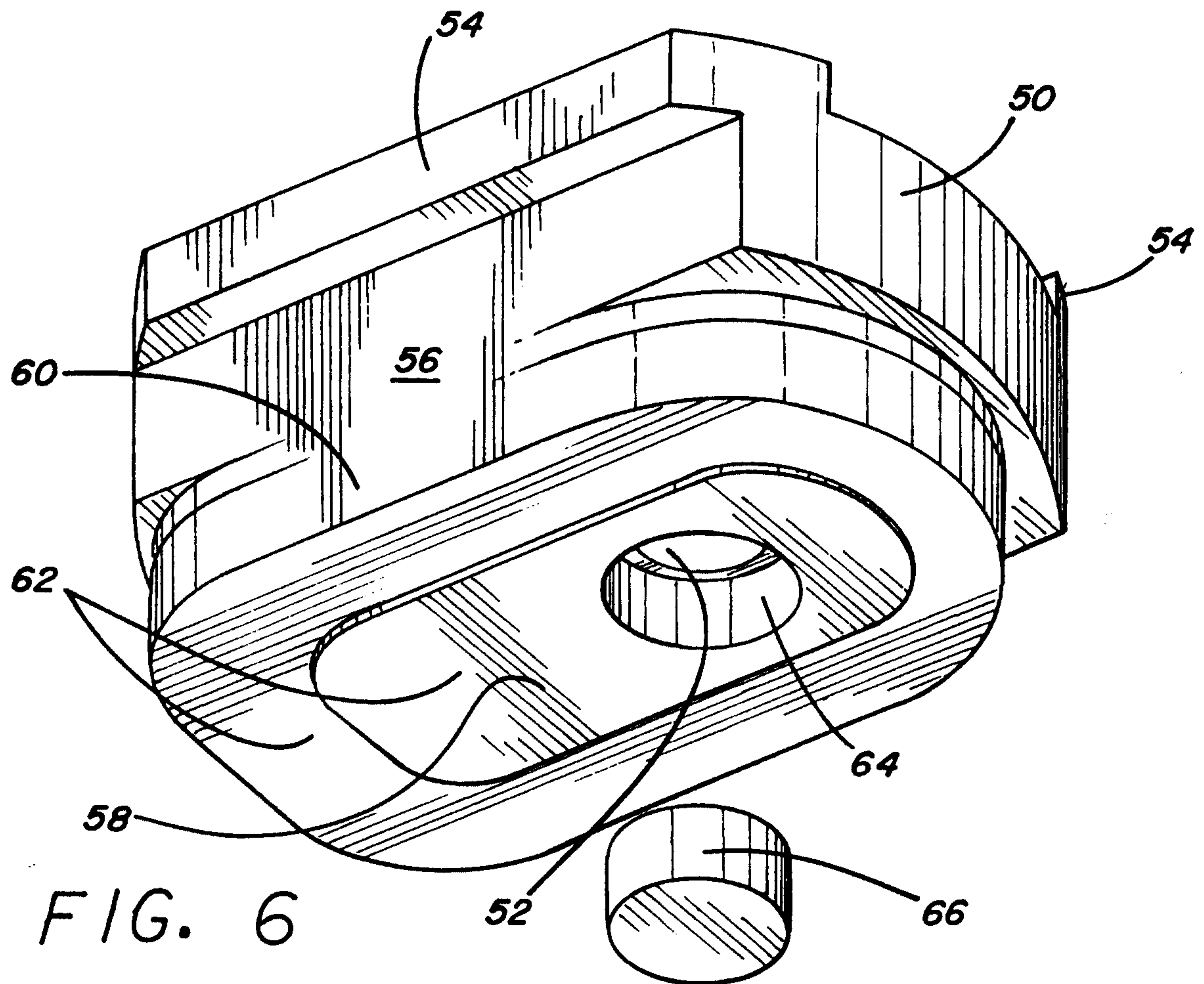


FIG. 3

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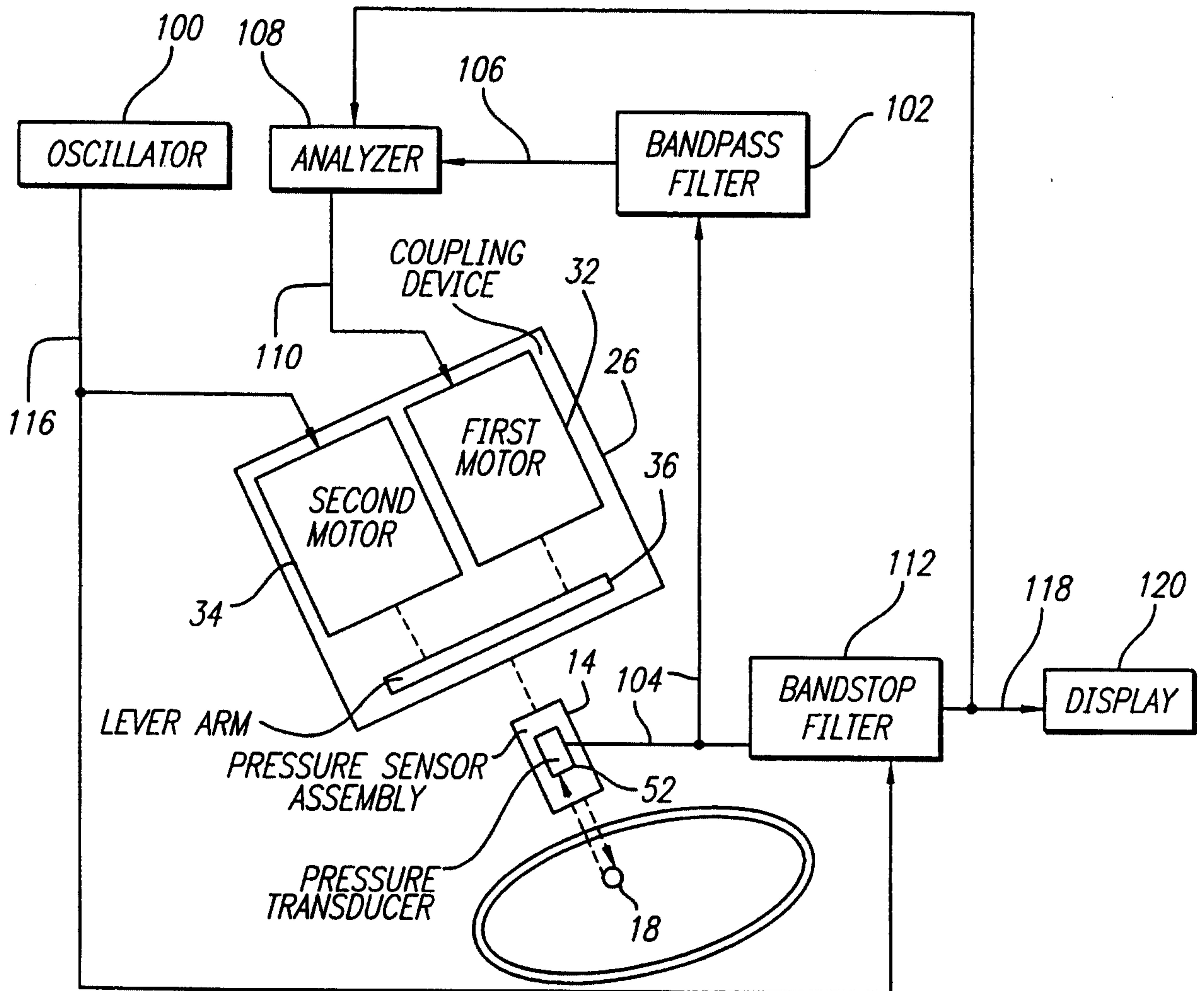


FIG. 8

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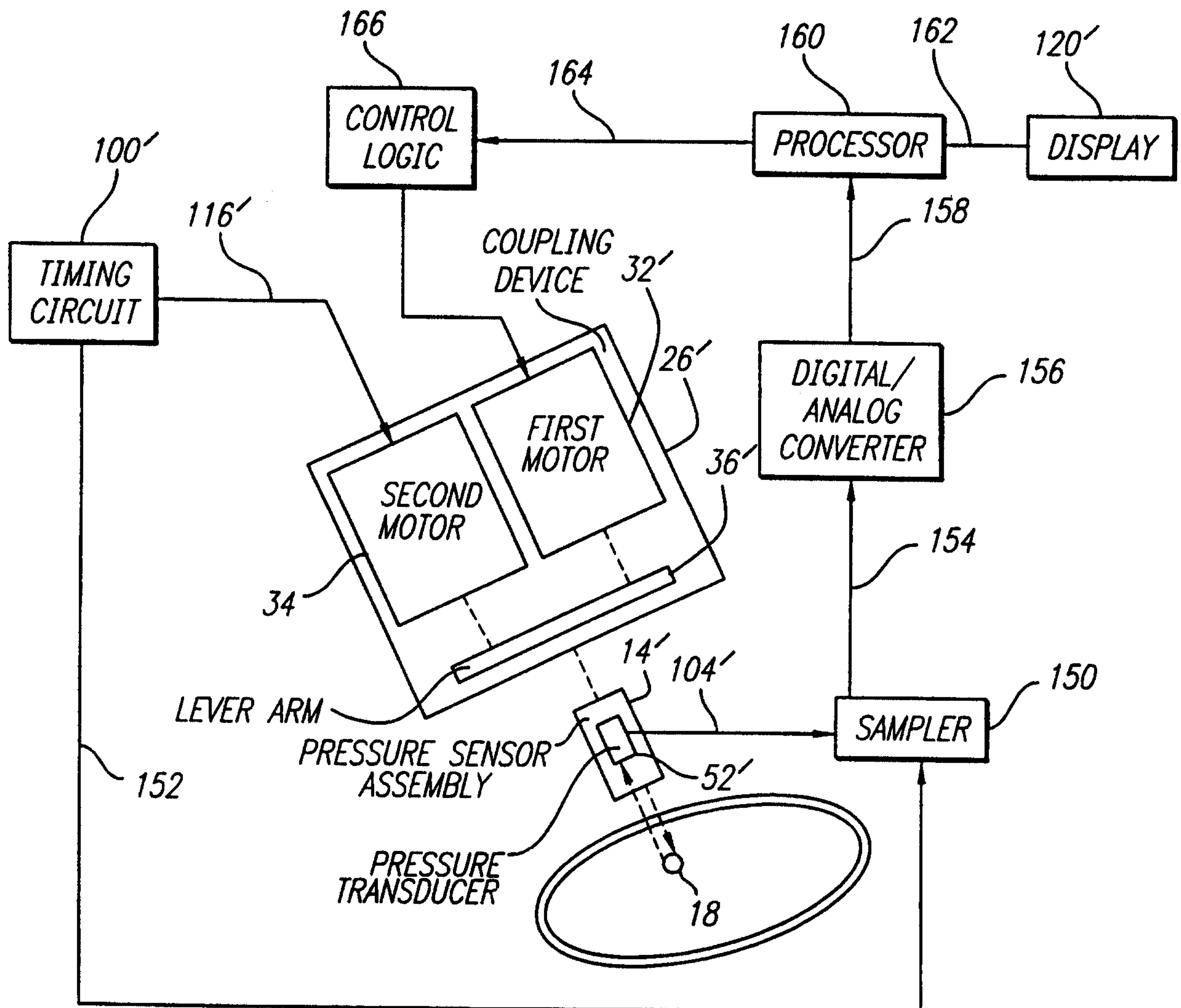


FIG. 9

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FIG. 10A

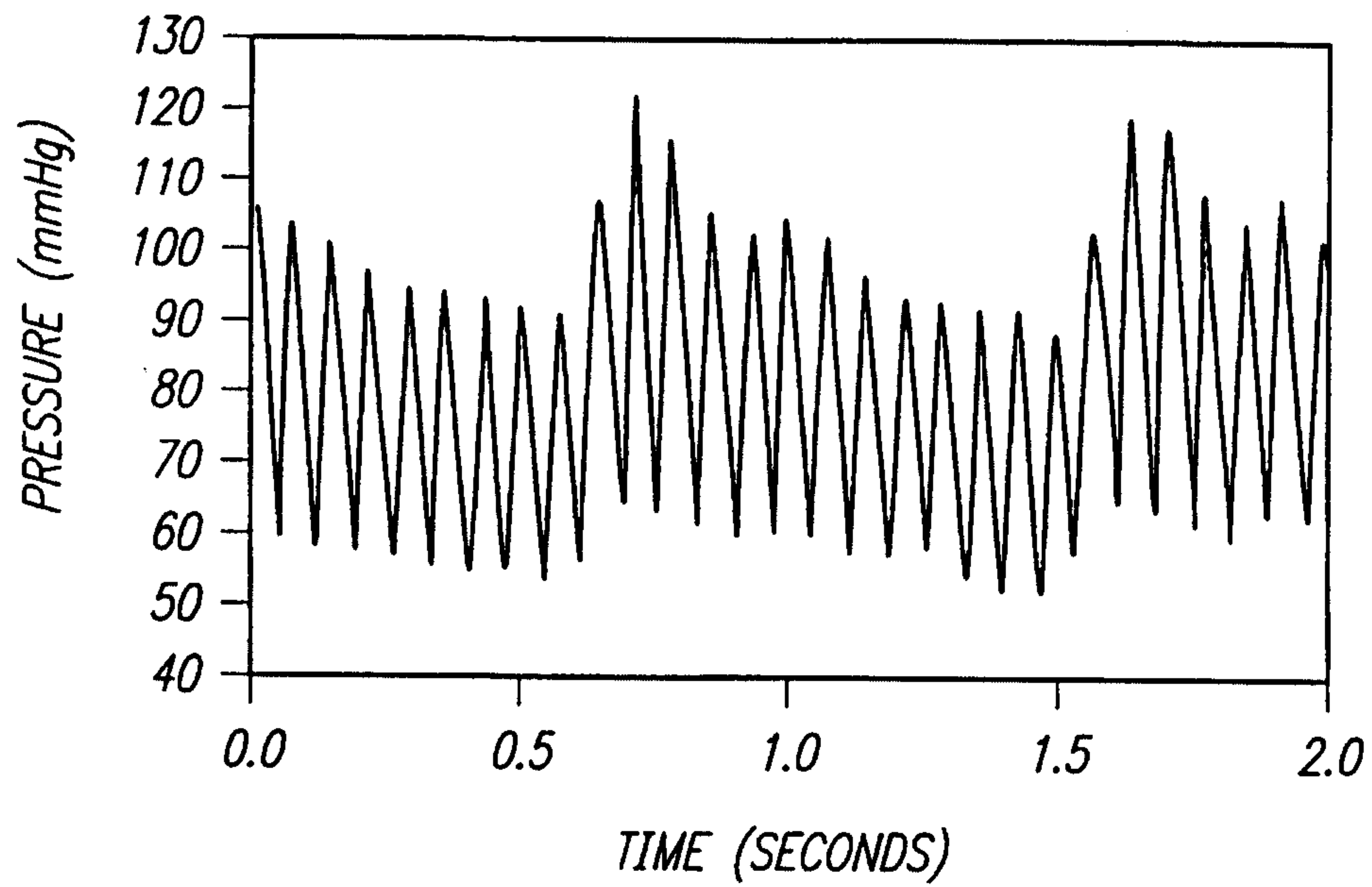
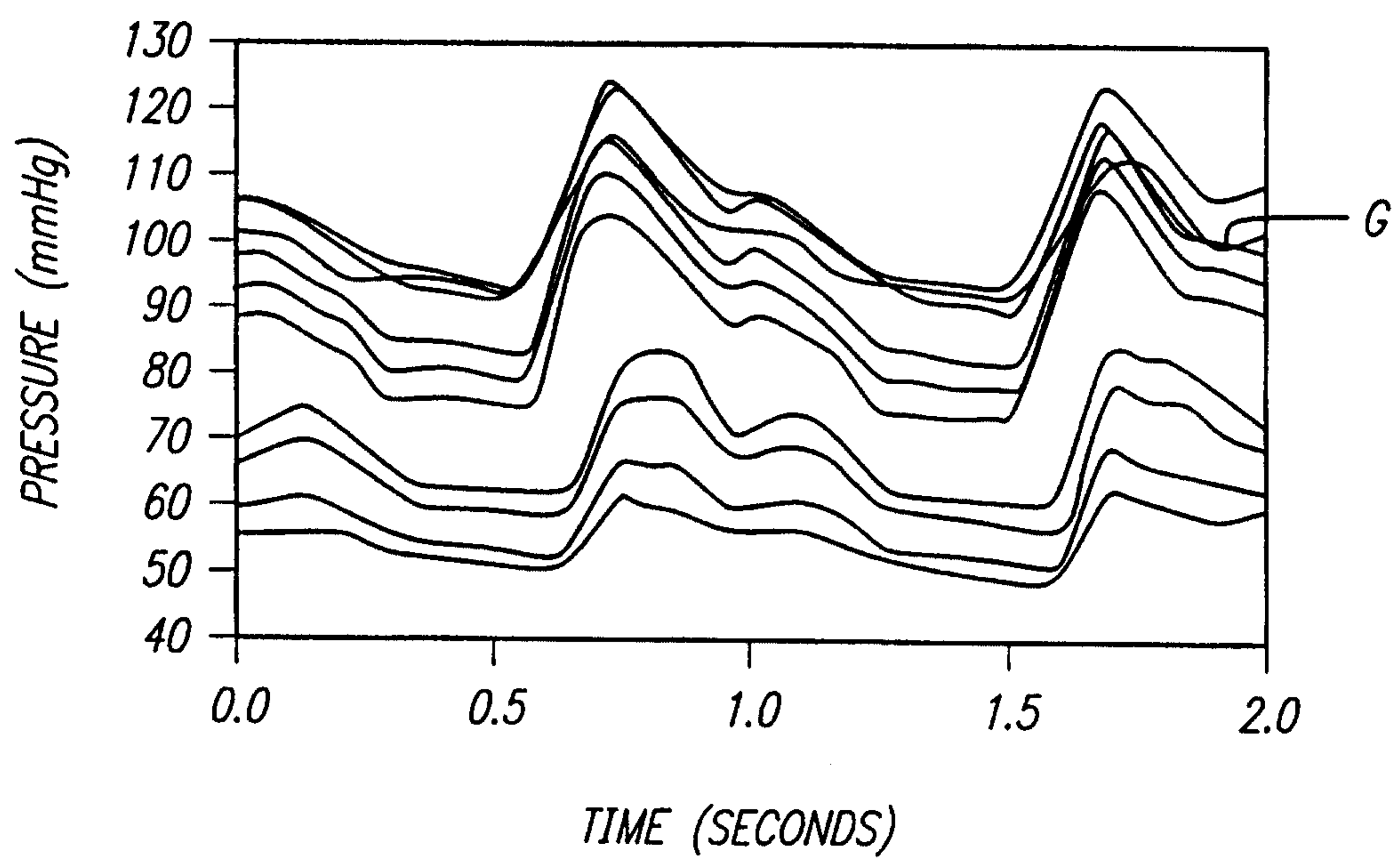


FIG. 10B



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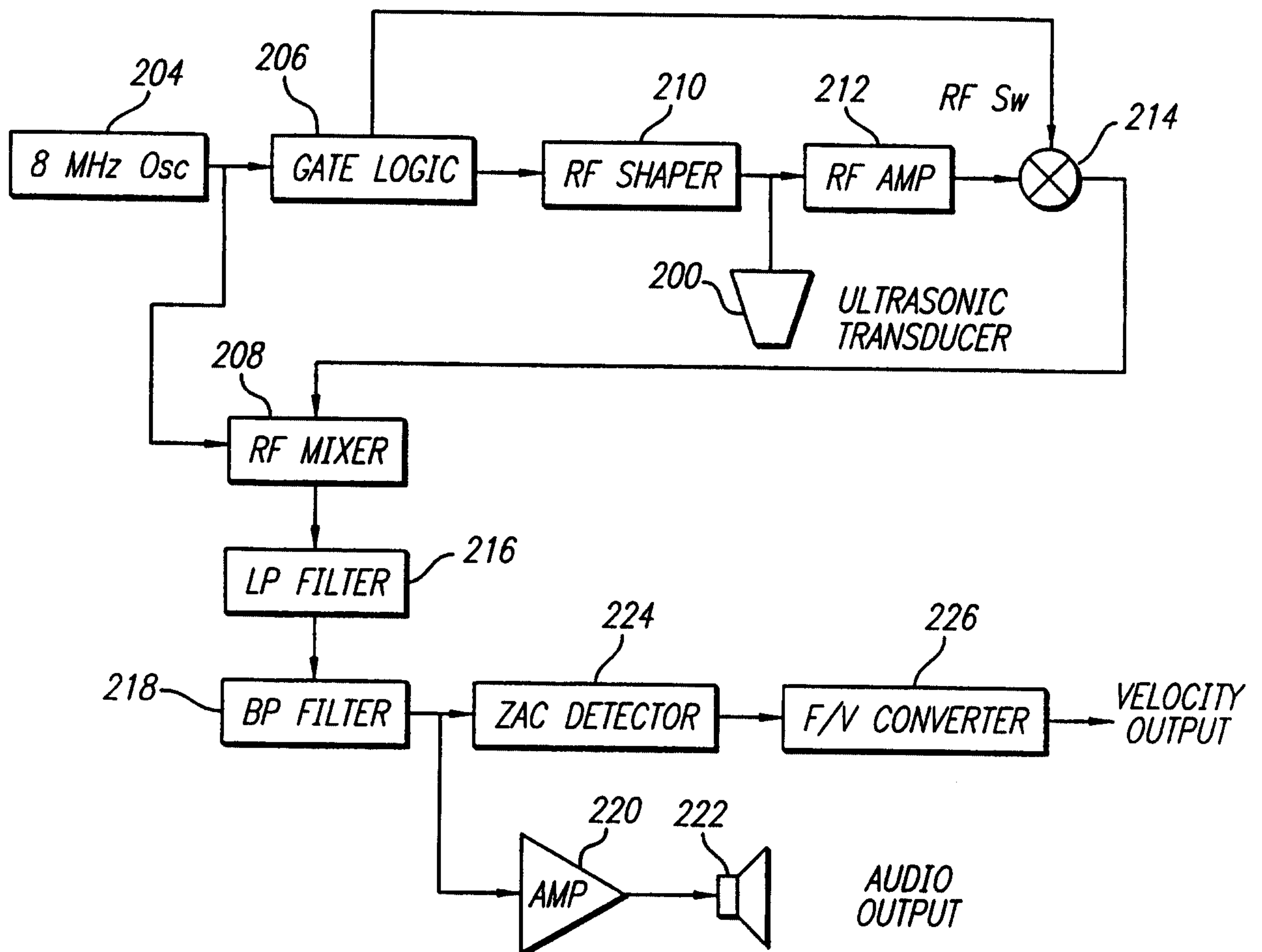


FIG. 11

