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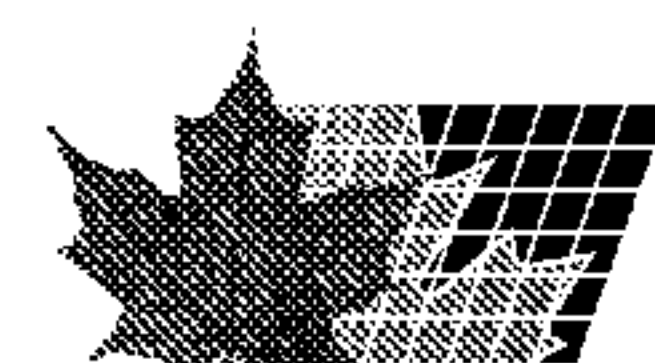
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(54) Titre : COMPOSITIONS ET PROCEDES POUR UTILISER DES CORPS LAMELLAIRES A DES FINS
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(54) Title: COMPOSITIONS AND METHODS OF USING LAMELLAR BODIES FOR THERAPEUTIC PURPOSES

(57) **Abrégé/Abstract:**

Compositions comprising therapeutically effective amounts of lamellar bodies for the modification of linear macromolecules are disclosed. These lamellar compositions are useful in the treatment of conditions or diseases characterized by a preponderance of heavy mucous secretions, such as otitis media, cystic fibrosis, bronchitis, sinusitis and nasal congestion. Methods of treating these diseases and conditions by administering a therapeutically effective amount of a composition to a patient requiring such treatment are also disclosed.



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(54) Title: COMPOSITIONS AND METHODS OF USING LAMELLAR BODIES FOR THERAPEUTIC PURPOSES

(57) Abstract: Compositions comprising therapeutically effective amounts of lamellar bodies for the modification of linear macromolecules are disclosed. These lamellar compositions are useful in the treatment of conditions or diseases characterized by a preponderance of heavy mucous secretions, such as otitis media, cystic fibrosis, bronchitis, sinusitis and nasal congestion. Methods of treating these diseases and conditions by administering a therapeutically effective amount of a composition to a patient requiring such treatment are also disclosed.

WO 2005/030226 A1

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9 COMPOSITIONS AND METHODS OF USING LAMELLAR BODIES FOR
10 THERAPEUTIC PURPOSES
11

12 The present invention relates to the identification of
13 lamellar bodies which modify linear biological
14 macromolecules that may be present in physiological and
15 pathophysiological secretions and exudates, such as
16 mucus, DNA, actin and bacterial-derived alginate, with
17 respect to their physical properties, viscosity,
18 adhesiveness, liquidity and three-dimensional
19 disposition. The invention further relates to
20 compositions and methods of treatment using these
21 lamellar bodies.
22

23 There are a number of occasions and sites where it would
24 be beneficial to modify linear biological macromolecules,
25 such as in disease states and during surgery. Examples
26 where linear macromolecules are problematic are acute and
27 chronic otitis media and sinusitis, acute and chronic
28 inflammatory disorders of the respiratory tract
29 (including cystic fibrosis), disorders of the alimentary
30 and genito-urinary tracts, and during surgical procedures
31 on ducts and surfaces of body cavities filled or covered

1 by thickened secretions or exudates. There are no
2 biologically efficacious substances or methods typically
3 used for alteration or removal of these species of
4 macromolecules, which in pathological situations can
5 result in acute and chronic morbidity and mortality.

6
7 On the simple basis of observed viscosity or lubricity,
8 older physiology texts classified secretions into thick
9 or thin. Thick secretions were described as "mucoid",
10 whereas thin secretions were considered "serous" in
11 nature. These ill-defined archaic terms are still in use
12 and have not been accurately defined and categorized. The
13 term "serous" is applied to the sparse, thin secretions
14 encountered universally in the large body cavities,
15 pleura, pericardium, peritoneum, joints and tendon
16 sheaths. This thin secretion is termed "serous" in that,
17 like serum, it does not clot. In the last decade however,
18 serous fluid in body cavities, was for the first time
19 accurately defined as a secretion of mesothelium in which
20 phospholipid microbodies were the predominant element in
21 conferring high lubricity and non-stick properties
22 (Dobbie JW, (1988) Ultrastructural similarities between
23 mesothelium and Type II pneumocytes and their relevance
24 to phospholipid surfactant production by the peritoneum
25 In: Khanna R, Nolph KD, Prowant B , Eds: Advances in
26 Continuous Ambulatory Peritoneal Dialysis. University of
27 Toronto Press, Toronto, pp 32-41; Dobbie JW, Pavlina T,
28 Lloyd J, Johnson RC. (1988); Am J Kid Dis., 12:31-36;
29 Dobbie JW, Lloyd JK. (1989), Perit Dial Int, 9:215-221).
30 Subsequently it has been shown that not only mesothelium
31 but many other tissues in respiratory, alimentary and
32 reproductive tracts contain varying densities of "serous"
33 cells, which secrete a similar substance.

1
2 Invisible to light and electron microscopy for so long,
3 these findings have recently been responsible for the
4 concept that the secretory system for these phospholipid
5 microbodies constitutes a hitherto unrecognized major
6 biological system throughout the animal kingdom (Dobbie
7 JW. (1996) Perit Dial Int. 16:574-581).

8
9 Widespread throughout the animal kingdom, the secretion
10 of mucus from body surfaces, in association with
11 underlying motile projections of cell surfaces, cilia,
12 together constitutes an important mechanical system for
13 automatic clearance of potentially noxious substances. In
14 lung, the mucociliary clearance system is the first line
15 of defence against inhaled particulates, aerosols and
16 pathogens, into its airways. Such materials are adsorbed
17 out of the air stream onto the mucous gel contained
18 within the airway surface liquid, which coats the
19 ciliated epithelium. Despite the focus of intensive
20 research in recent years, particularly in relation to the
21 pathogenesis of cystic fibrosis, there remain unsolved
22 biophysical problems in understanding the function of
23 mucociliary clearance in all body surfaces. It is with
24 respect to the identification of compositions for the
25 treatment of diseases and conditions characterized by the
26 preponderance of thick mucous secretions that the present
27 application is directed.

28
29 The present invention relates to the discovery that
30 lamellar body secretory cells are a biological necessity
31 in sites where thick secretions such as mucus are
32 produced, and in disease states where linear

1 macromolecules possessing significant inherent visco-
2 elastic and adhesive properties might be encountered.

3

4 It would be beneficial to provide a substance or method
5 that is able to modify for therapeutic purposes linear
6 macromolecules with respect to their physical properties
7 in relation to viscosity, adhesiveness and rheological
8 characteristics.

9

10 Accordingly, a first aspect of the present invention
11 provides for a composition comprising a therapeutically
12 effective amount of lamellar bodies for the modification
13 of linear macromolecules. In a preferred embodiment, the
14 composition is a pharmaceutical composition comprising
15 the lamellar bodies and a pharmaceutically acceptable
16 carrier. In another preferred embodiment, the
17 pharmaceutical compositions may be used to treat a
18 mammalian subject suffering from a disease or condition
19 characterized by a preponderance of heavy mucous
20 secretions and in need of such therapy. Such conditions
21 include, but are not limited to, Otitis Media (acute or
22 chronic), Cystic Fibrosis, sinusitis, bronchitis, and
23 nasal congestion. In another preferred embodiment, the
24 subject is a human. In another preferred embodiment, the
25 lamellar bodies comprise about 44-70%
26 phosphatidylcholine, about 15-23% sphingomyelin, about 6-
27 10% phosphatidyl ethanolamine, about 2-6% phosphatidyl
28 serine, about 2-4% phosphatidyl inositol and about 4-12%
29 cholesterol by weight. In another preferred embodiment,
30 the composition further comprises about 0-3% by weight of
31 lysophosphatidyl choline. In a further preferred
32 embodiment, the lamellar bodies comprise about 54%
33 phosphatidylcholine, about 19% sphingomyelin, about 8%

1 phosphatidyl ethanolamine, about 4% phosphatidyl serine,
2 about 3% phosphatidyl inositol and about 10% cholesterol
3 by weight. In another preferred embodiment, the
4 composition further comprises about 2% by weight of
5 lysophosphatidyl choline. In yet another preferred
6 embodiment, the linear macromolecules in need of
7 modification are selected from the group consisting of
8 DNA, mucin, actin, and bacterial-derived alginate. These
9 substances may be produced by the host or invading micro-
10 organisms, i.e. they are substances produced or released
11 by either prokaryotes or eukaryotes.

12
13 A second aspect of the present invention provides for a
14 method of treatment for acute and chronic otitis media.
15 In a preferred embodiment, the method of treatment
16 comprises the steps of:

- 17 a) inserting a needle through the tympanic
18 membrane;
19 b) introducing a composition including lamellar
20 bodies through the needle into the ear; and
21 c) allowing the lamellar bodies to modify the
22 viscosity of the mucin in the ear such that it is
23 capable of draining from the ear.

24
25 In another preferred embodiment, the method of treatment
26 of otitis media comprises the steps of:

- 27 a) inserting a needle through the tympanic
28 membrane;
29 b) introducing a composition including lamellar
30 bodies through the needle into the ear; and
31 c) allowing the lamellar bodies to modify the
32 composition and the biological properties of the
33 contents present in the pathological secretion,

1 including linear macromolecules of the type mucus,
2 DNA, actin and alginate, to the effect that the
3 physical properties of the secretions such as
4 viscosity and adhesiveness are altered, permitting
5 therapeutic drainage of the middle ear.
6

7 In another preferred embodiment, the method of treating
8 otitis media where a tympanostomy tube (vent tube) is in
9 place and has become blocked by mucus or by an admixture
10 of mucus and DNA, actin, alginate or wax, comprises the
11 step of introducing a composition including lamellar
12 bodies into the external auditory canal.
13

14 In yet another preferred embodiment, the method of
15 treatment for otitis media comprises the steps of :

- 16 a) inserting a catheter into the pharyngeal opening of
17 the Eustachian tube.
18 b) introducing a composition, including lamellar bodies
19 through the catheter into the ear.
20

21 Preferably the composition is introduced into the middle
22 ear.
23

24 A third aspect of the present invention provides for a
25 method of performing a functional endoscopic sinus
26 surgical (FESS) procedure on the sinus or sinuses of a
27 patient comprising the steps of:

- 28 a) applying a composition including lamellar bodies to
29 the sinus or sinuses;
30 b) allowing lamellar bodies in the composition to
31 modify the physical properties of viscosity and
32 adhesiveness of linear macromolecules, including
33 mucus, DNA, actin and alginate in the area of the

1 sinus or sinuses such that the substances are capable
2 of being removed; and
3 c) introducing a surgical instrument into the nasal
4 passage such as to remove tissue from the sinus or
5 sinuses.

6
7 A fourth aspect of the present invention provides for a
8 method for applying a composition including lamellar
9 bodies to the respiratory passages to modify the physical
10 properties of linear macromolecules of the type mucus,
11 DNA, actin and alginate in pathologically altered
12 secretions. The lamellar bodies modify the viscosity and
13 adhesiveness of the secretions, increasing the fluidity
14 of the airways' surface fluid and restoring mucociliary
15 clearance of secretions throughout the respiratory tract.
16 In a preferred embodiment, the composition containing
17 suspended lamellar bodies is introduced into the
18 respiratory passages as an aerosol spray. In another
19 preferred embodiment, the fluid containing suspended
20 lamellar bodies may be subjected to ultrasonification
21 during administration of inhaled aerosol. In yet another
22 preferred embodiment, the therapeutic moieties can be
23 included on or within the phospholipid bilayers which
24 constitute the lamellar bodies for more effective access
25 of therapeutic moieties to sequestered micro-organisms
26 protected by prokaryote- and eukaryote-derived linear
27 macromolecules.

28
29 A fifth aspect of the present invention provides for a
30 method for applying a composition, including lamellar
31 bodies, to diverse parts of the body for the symptomatic
32 relief of viscous secretions in patients with the
33 autosomal recessive disorder, cystic fibrosis, due to the

1 gene defect responsible for the secretion of a protein
2 called Cystic Fibrosis Transmembrane Conductance
3 Regulator (CFTR). In a preferred embodiment, the method
4 of symptomatic treatment of the pathological secretions
5 in cystic fibrosis is accomplished by applying a
6 composition containing suspended lamellar bodies which
7 are introduced into the respiratory passages as an
8 aerosol spray. In another preferred embodiment, the fluid
9 containing suspended lamellar bodies may be subjected to
10 ultrasonification during administration of inhaled
11 aerosol. In yet another preferred embodiment, additional
12 therapeutic moieties can be included on or within the
13 phospholipid bilayers which constitute the lamellar
14 bodies for more effective access of the therapeutic
15 moieties to sequestered micro-organisms protected by
16 prokaryote- and eukaryote-derived linear macromolecules.
17 Another preferred embodiment provides for a method of
18 symptomatic treatment of the effects of blockage of the
19 secretory ducts of vital organs and glands in patients
20 with cystic fibrosis by applying a composition including
21 lamellar bodies through intermittent or continuous
22 infusion into the drainage system by needles or
23 appropriate macro- or micro-catheters, or introduction of
24 slow-release matrices, enteric-coated or biodegradable
25 capsules containing lamellar bodies.

26
27 Other advantages of the present invention will become
28 apparent from the ensuing detailed description taken in
29 conjunction with the following illustrative drawings.

30
31 In order to provide a better understanding of the present
32 invention, embodiments and uses of the invention will now

1 be described by way of example only and with reference to
2 the following Figures.

3

4 **Figure 1.** Effect of varying concentrations of synthetic
5 lamellar bodies on mucus fluidity compared with use of
6 saline diluent as control. Each sample tested was
7 exactly 30 μ l. The angle of incline was 90°.

8

9 **Figure 2.** Effect at 37°C of varying concentrations of
10 synthetic lamellar bodies on DNA fluidity compared with
11 use of saline diluent as control. Each sample tested was
12 100 μ l. The angle of incline was 90°.

13

14 **Figure 3.** Effect at 37°C of synthetic lamellar bodies on
15 fluidity of a combined mucus - DNA gel at a ratio of one
16 third volume synthetic lamellar bodies to two thirds DNA
17 & mucus gel compared with control using one third volume
18 of 0.9% saline. Each sample tested was 40 μ l. The angle
19 of incline was 90°.

20

21 Before the present methods and treatment methodology are
22 described, it is to be understood that this invention is
23 not limited to particular methods, and experimental
24 conditions described, as such methods and conditions may
25 vary. It is also to be understood that the terminology
26 used herein is for purposes of describing particular
27 embodiments only, and is not intended to be limiting,
28 since the scope of the present invention will be limited
29 only in the appended claims.

30

31 As used in this specification and the appended claims,
32 the singular forms "a", "an", and "the" include plural
33 references unless the context clearly dictates otherwise.

1 Thus, for example, references to "the method" include one
2 or more methods, and/or steps of the type described
3 herein and/or which will become apparent to those persons
4 skilled in the art upon reading this disclosure and so
5 forth.

6
7 Unless defined otherwise, all technical and scientific
8 terms used herein have the same meaning as commonly
9 understood by one of ordinary skill in the art to which
10 this invention belongs. Although any methods and
11 materials similar or equivalent to those described herein
12 can be used in the practice or testing of the invention,
13 the preferred methods and materials are now described.
14 All publications mentioned herein are incorporated herein
15 by reference in their entirety.

16
17 **"Lamellar bodies or microbodies"** as used throughout this
18 document, refers to phospholipid, multilamellar,
19 bilayered structures present in many tissues throughout
20 the body, but also refers to the synthetic multilayered
21 phospholipid structures having the novel composition
22 described in the present invention. Thus, this term
23 refers to both naturally occurring and synthetic lamellar
24 bodies.

25
26 **"Lamellasomes"** as used herein refers to synthetically
27 prepared lamellar bodies as described by the methods of
28 the present invention.

29
30 **"Serous"** as used herein refers to an exudate or effusion
31 that is thin and watery, and which lacks a significant
32 cellular component.

1 **"Treat", Treating"** or **"Treatment"** refers to therapy,
2 prevention and prophylaxis and particularly refers to the
3 administration of medicine or the performance of medical
4 procedures with respect to a patient, for either
5 prophylaxis (prevention) or to cure or reduce the extent
6 of or likelihood of occurrence of the infirmity or malady
7 or condition or event in the instance where the patient
8 is afflicted.

9
10 A **"therapeutically effective amount"** is an amount
11 sufficient to decrease or prevent the symptoms associated
12 with the conditions or deficiencies contemplated for
13 therapy with the compositions of the present invention.

14
15 **"Slow release formulation"** refers to a formulation
16 designed to release a therapeutically effective amount of
17 a drug or other active agent such as a polypeptide or a
18 synthetic compound over an extended period of time, with
19 the result being a reduction in the number of treatments
20 necessary to achieve the desired therapeutic effect. In
21 the matter of the present invention, a slow release
22 formulation would decrease the number of treatments
23 necessary to achieve the desired effect.

24
25 **"Combination therapy"** refers to the use of the agents of
26 the present invention with other active agents or
27 treatment modalities, in the manner of the present
28 invention for treatment of otitis media or abdominal
29 surgery. These other agents or treatments may include
30 drugs such as corticosteroids, non-steroidal anti-
31 inflammatory compounds, or other agents useful in
32 treating or alleviating pain. The combined use of the
33 agents of the present invention with these other

1 therapies or treatment modalities may be concurrent, or
2 the two treatments may be divided up such that the agent
3 of the present invention may be given prior to or after
4 the other therapy or treatment modality.

5
6 **"Local administration"** means direct administration by a
7 non-systemic route at or in the vicinity of the site of
8 an affliction, disorder, or perceived pain.

9
10 **"Modify" or "modification of"** means to alter the physical
11 status of a material with respect to viscosity,
12 adhesiveness and/or fluidity. In the present invention
13 "modification" refers to changes in physical
14 characteristics, perhaps due to changes in hydration of
15 the gel, although other factors may play a role in
16 modification of the physical state.

17
18 **"Acute otitis media"** is an inflammation of the area
19 behind the eardrum (tympanic membrane) in the chamber
20 called the middle ear. Acute otitis media is an infection
21 that produces pus, fluid, and inflammation within the
22 middle ear. Acute otitis media frequently occurs as an
23 after-effect of respiratory infections as the nasal
24 membranes and eustachian tube become swollen and
25 congested.

26
27 **"Chronic otitis media"** refers to a middle ear infection
28 that may develop when infection in the middle ear
29 persists for more than 2 weeks. The middle ear and
30 eardrum may start to sustain ongoing damage occasionally
31 resulting in drainage through a nonhealing hole in the
32 eardrum.

1 Throughout this document the term "linear macromolecule"
2 refers to molecules which are linear at the molecular
3 level and whose structure essentially comprises the
4 multiple repetition in linear sequence of units derived
5 from molecules of low relative molecular mass. The
6 molecules may possess side-chains, but these will not
7 typically participate in chemical cross-linking.
8 Examples of linear macromolecules of this species include
9 mucus, DNA, actin and alginate.

10 "Therapeutic moieties" refers to any therapeutically
11 effective molecule, whether it is a small organic
12 chemical compound, or a protein or peptide, or a nucleic
13 acid, or an antibody or antibody fragment, or a
14 carbohydrate, that may be attached to the lamellar bodies
15 and administered to subjects suffering from diseases or
16 conditions for which treatment may be beneficial.
17 Optionally, therapeutic moieties can be included on or
18 within the phospholipid bilayers which constitute the
19 lamellar bodies.

20
21 It was not until the time of the present invention that
22 treatment of diseases having thick mucoid secretions with
23 compositions containing the lamellar bodies of the
24 present invention was contemplated. That is, a recent key
25 advance in molecular biology and physiology has been the
26 realisation that the thin "serous" secretions which have
27 high lubricity and do not form gels (clots), can exist on
28 their own in body cavities, ducts, glands, surfaces, etc,
29 whereas thick, "mucoid" secretions are in normal
30 physiological states always accompanied by cells which
31 secrete a serous solution containing phospholipid
32 microbodies.

1 The invention described herein has provided new
2 observations and explanatory concepts resulting in the
3 conclusion that a biological agent which counteracts the
4 viscosity of thick mucous secretions is always provided
5 in the form of accompanying "serous" secretory cells. The
6 likeliest function of phospholipid microbodies on gels
7 consisting of tangled linear polymers would be the
8 modification of their adhesive and visco-elastic
9 properties.

10
11 Studies on the effect of synthetic lamellar bodies on the
12 adhesiveness, viscosity and fluidity properties of mucous
13 secretions has for the first time provided observations
14 that the key constituents of "serous" secreting cells
15 (lamellar bodies) significantly modify the physical
16 properties of mucus. It has further been shown that
17 synthetic lamellar bodies also have a significant effect
18 on the physical properties of pathophysiological thick
19 secretions, which contain polymeric DNA, actin or
20 alginate derived from dead host cells and bacteria.

21 22 **Therapeutic Uses and Compositions**

23 **Chronic otitis media with effusion (COME)**

24 COME is an extremely common condition, particularly in
25 children. Following an acute or repeated acute attacks of
26 otitis media, the middle ear may become filled with a
27 viscous secretion referred to as "glue ear". This can
28 become an intractable problem with serious consequences
29 for hearing and in many cases, delayed or impaired speech
30 and learning. Venting through grommets is the mainstay
31 of present-day practice. There is widespread agreement
32 among otolaryngologists that current methods of treatment
33 are often sub-optimal in their outcome. Although much

1 recent effort has been deployed into research to find
2 better modes of treatment, it is unfortunate that only
3 minimal attention has been paid to the little known
4 finding of serous secreting cells in the Eustachian tube
5 and middle ear.

6

7

8 **Nature of the epithelial lining of the middle ear and the**
9 **Eustachian tube**

10 The nature of the lining of the Eustachian tube and
11 middle ear has for long been considered to be a
12 "modified" respiratory epithelium containing both
13 ciliated and goblet cells derived from the basal layers.
14 However, based on investigations of whole mounted
15 histological preparations from fetuses, premature
16 infants, infants, normal children and adults, Tos
17 concluded that mucous secreting cells are not a normal
18 but a pathological component of middle ear epithelium
19 (Tos M, Caye-Thomasen P, (2002), J Oto-Rhino-Laryngology
20 & Related Specialities. 64:86-94). Indeed, it is now
21 increasingly accepted that the lining epithelium
22 throughout the Eustachian tube and middle ear in normal
23 health, secretes but a sparse, thin solution which merely
24 confers a glistening appearance to the membrane. The only
25 cells likely to be responsible are loosely described in
26 the literature as "serous" cells.

27

28 **Aetiopathogenesis of chronic otitis media with effusion**
29 **(COME)**

30 It is now accepted that the key factor in the
31 aetiopathogenesis of COME is the metaplastic
32 transformation of middle ear epithelium to a
33 predominantly goblet cell layer engaged in long-term

1 hypersecretion of mucus. Recent research into the
2 pathophysiology of COME has demonstrated a continuous
3 chain of reactions precipitated by bacterial infection,
4 where stimulation by endotoxins, together with pro-
5 inflammatory cytokines (IL1 β , TNFa, IL8, PAF) and growth
6 factors (ErbB & HepGF) are not only powerful promoters of
7 goblet cell hyperplasia, but also act as highly potent
8 secretagogues of mucus.

9

10 **Functions of lamellar body secretory system**

11 In pulmonary alveoli the prime function of lamellar
12 bodies is the provision of surfactant phospholipids to
13 promote gaseous exchange at the fluid-air interface, and
14 to lower the opening pressure of alveolar walls during
15 inspiration.

16

17 In mesothelial-lined cavities, we have shown the function
18 of lamellar bodies to be that of lubrication and
19 provision of a non-stick surface. This is achieved
20 through the formation of microscopic, multilamellar ball
21 and roller bearings which constantly form and reform
22 between sliding surfaces.

23

24 In open body surfaces and ducts, upper respiratory,
25 gastro-intestinal and reproductive tracts, we have
26 produced evidence that, in addition to conferring non-
27 stick properties, a key function of lamellar body
28 secretion in these sites is the modification and/or
29 disaggregation of locally produced gels, such as mucus.
30 This extremely important property is the biological
31 guarantee that vital surfaces, ducts and tubes have a
32 highly conserved method for preventing smothering and
33 blockage by viscous secretions.

Lamellar body secretion in middle ear

In 1984 it was first demonstrated that the epithelial lining of the rat Eustachian tube synthesised phosphatidylcholine, the principal constituent of pulmonary surfactant, in amounts comparable to that produced by pulmonary alveolar epithelium (Wheeler SL, Pool GL, Lumb RH. (1984), Biochim Biophys Acta, 794:348-349). This was the first indication that the Eustachian tube epithelium produced a secretion with surfactant properties. Although this paper stimulated Dobbie et al (Dobbie JW, Pavlina T, Lloyd J, Johnson RC, (1988), Am J Kid Dis, 12:31-36) to apply their methodology to mesothelium, Wheeler's pioneering observations failed to evoke much interest or research in the otolaryngological community. In the last several years however, a small number of research papers on the ultrastructure of middle ear epithelium has confirmed by electron microscopy the presence of lamellar body secreting cells, so-called "serous" cells (Mira E, Bonazzo M, Galioto P et al. (1988), J Auto-rhino Laryngology & Related Specialities, 50:251-256.).

New concepts on the function of phospholipid secretion in normal state and pathological conditions in middle ear

A review of recent research carried out on the epithelial lining of the middle ear, considered in relation to our comparative ultrastructural and physiological research on lamellar body secretion at all other non-pulmonary locations, indicates that in the normal state, a constant thin secretion of lamellar bodies has a prime function in providing a non-stick surface in the Eustachian tube, tympanic cavity and air sacs, as we have demonstrated in

1 the mesothelial-lined cavities of the body. In this site
2 formation of adhesions, synechiae or outright blockage of
3 the ductal portions of the system must be avoided at all
4 costs. Thus it would have been surprising indeed if the
5 benefit of highly conserved non-stick properties of
6 lamellar bodies had not been present in these important
7 cavities.

8
9 Like the upper respiratory tree, the middle ear, under
10 the stimulus of inflammation, has the ability to produce
11 mucous secreting goblet cells. However, current
12 understanding of the physiology and pathophysiology of
13 middle ear has not yet become aware of the dual, balanced
14 system of mucus and lamellar body secretion.

15
16 The preparation of synthetic lamellar bodies now allows,
17 for the first time, an opportunity to examine the
18 interaction in a controlled ex vivo model, the possible
19 physico-chemical interaction between phospholipid
20 microbodies and naturally-occurring gels consisting of
21 tangled networks of linear glycoprotein polymers.

22 23 **"Surfactant" in the middle ear**

24 In the last several years there has been a quickening of
25 interest in the possible role of "surfactant" in the
26 physiology and pathophysiology of the middle ear. The
27 theme of the investigations has assumed that surfactants
28 are in some way involved with ventilation, protection and
29 clearance of the middle ear through the Eustachian tube.
30 These functions have been examined by administration of
31 exogenous surfactant and have successfully demonstrated
32 that surfactant decreased the opening forces of the
33 Eustachian tube, even in otologically healthy rats (Van

1 Heerbeek N, Tonnaer ELGM, Koen JAO et al. (2003), Otology
2 & Neurotology, 24: 6-10). In this capacity however, the
3 lamellar bodies supplied in the surfactant are not
4 functioning as a surfactant as such, but as a coating,
5 which prevents adhesion of opposing surfaces. No
6 significant effect however was observed on mucociliary
7 clearance. In this respect there is an on-going failure
8 to recognise that it is now established that the
9 lubricating and non-stick properties of lamellar bodies
10 constitute the major function of this system, and its
11 pulmonary surfactant properties are a late, highly
12 specialised evolutionary development. Similarly, it has
13 not yet dawned on workers in this field that it would be
14 a worthwhile experiment to mix these lubricating
15 microbodies with gels of linear macromolecules such as
16 mucus and DNA, which are pivotal in middle ear pathology.

17
18 This is not to deny the importance of the lamellar
19 bodies' role as a surfactant in the gaseous exchange
20 which occurs across the middle ear and associated air
21 cells, and must play some significant part in
22 ventilation. This well-known function of surfactant
23 however, has blind-sighted researchers from investigating
24 the more mundane role of lamellar bodies as a "biological
25 lubricant and cleanser" of thick secretions.

26
27 **Secretion of lamellar bodies by serous cells in the**
28 **mucosa of the nasal cavities and sinuses**

29 It has recently been shown that there are scattered
30 throughout these cavities serous cells which have been
31 shown by electron microscopy to secrete typical lamellar
32 bodies. In chronic infection, under the stimulus of
33 endotoxins, exotoxins, and pro-inflammatory cytokines,

1 there is a hyperplasia of goblet cells leading to
2 excessive mucous secretion. These cavities are then
3 liable to blockage and interruption of drainage due to
4 thick secretions of viscous mucus, DNA, actin and
5 bacterial-derived alginate.
6
7 Therapeutic application of lamellar bodies by aerosol
8 spray typically will be used in disorders of the
9 respiratory passages in which pathophysiological changes
10 in the consistency of secretions due to alterations in
11 concentration and/or physical status of linear
12 macromolecules are acute and chronic organismal-induced
13 inflammation of the respiratory passages (acute and
14 chronic bronchitis, bronchiectasis etc), acute and
15 chronic inflammation induced by allergens (organic and
16 inorganic) as in all types of asthma. Increased viscosity
17 of secretions caused by inhalation of irritant or toxic
18 particulate inducing alteration in the thickness of
19 airway secretions as in for example, byssinosis due to
20 inhalation of cotton dust and bagassosis, inhalation of
21 bagasse (dried sugar cane refuse). The application of
22 lamellar bodies will also be made to the respiratory
23 passages to disperse extracellular polymeric substance
24 (EPS), a protective biofilm secreted by diverse
25 pathogenic micro-organisms, including Pseudomonas
26 aeruginosa, in chronic respiratory disorders.

27

28 Use of Lamellar Bodies to Treat Cystic Fibrosis

29 The present invention also provides for a method for
30 applying a composition, including lamellar bodies, to
31 diverse parts of the body for the symptomatic relief of
32 viscous secretions in patients with the autosomal
33 recessive disorder, cystic fibrosis, due to the gene

1 defect responsible for the secretion of a protein called
2 Cystic Fibrosis Transmembrane Conductance Regulator
3 (CFTR). This renders the cell membrane permeant to
4 chloride and other larger organic anions. The condition
5 is characterized by gross increases in the concentration
6 and viscosity of mucus in the respiratory, alimentary,
7 gastro-intestinal and reproductive tracts. Chronic, high
8 density colonization of secretions by bacteria, leads to
9 sequestration of high concentrations of polymeric DNA and
10 actin from dead host leucocytes and bacteria which
11 further thicken the secretions, paralysing mucociliary
12 clearance. Also, colonization by organisms which actively
13 secrete protective biofilms including Pseudomonas
14 aeruginosa which produce a viscous linear macromolecule
15 (alginate), further thickening pathological secretions
16 and creating physical barriers, rendering the organism
17 inaccessible to chemotherapeutic attack. In cystic
18 fibrosis, respiratory disease is the principal cause of
19 mortality.

20
21 There are no biologically efficacious substances or
22 methods typically used for modifying the physical
23 properties these species of linear macromolecules which,
24 in concert, are responsible for dysfunctional secretions
25 in cystic fibrosis.

26
27 The present invention provides for a method of
28 symptomatic treatment of the pathological secretions in
29 cystic fibrosis by applying a composition containing
30 suspended lamellar bodies which are introduced into the
31 respiratory passages as an aerosol spray. Optionally, the
32 fluid containing suspended lamellar bodies may be

1 subjected to ultrasonification during administration of
2 inhaled aerosol.

3
4 Optionally, therapeutic moieties can be included on or
5 within the phospholipid bilayers which constitute the
6 lamellar bodies for more effective access of therapeutic
7 moieties to attack sequestered micro-organisms protected
8 by prokaryote- and eukaryote-derived linear
9 macromolecules.

10
11 Although pathological secretions in the respiratory tract
12 are the principal cause of morbidity and mortality, their
13 effect on other surfaces, passages and ducts results in
14 significant lesions due to blockage and cyst formation
15 particularly in the alimentary and genito-urinary tracts
16 in patients with CF. As for the respiratory tract, there
17 are no biologically efficacious substances or methods
18 typically used in cystic fibrosis for modifying the
19 effects of linear macromolecules in extrapulmonary sites.

20
21 The present invention also provides for a method of
22 symptomatic treatment of the effects of blockage of the
23 secretory ducts of vital organs and glands in patients
24 with cystic fibrosis by applying a composition including
25 lamellar bodies through intermittent or continuous
26 infusion into the drainage system by needles or
27 appropriate macro- or micro-catheters, or introduction of
28 slow-release matrices, enteric-coated or biodegradable
29 capsules containing lamellar bodies.

30
31 This method of symptomatic treatment is appropriate for
32 ductal structures and passages throughout the entire
33 body, including the surfaces of the gastro-intestinal

1 tract with particular relevance to the thickened membrane
2 covering the mucosa of the small bowel, pancreatic and
3 hepato-biliary drainage network, the genito-urinary
4 system, including intra-renal tubules, medullary drainage
5 system, renal pelvis, ureters, bladder, bladder
6 diverticula, urethra, vesico-colic fistula, ileo-vesicle
7 fistula, vas deferens, seminal vesicles, prostate,
8 cervix, endometrium, Fallopian tube mucosa, salivary and
9 lachrymal glands.

10
11 Optionally, therapeutic moieties can be included on or
12 within the phospholipid bilayers which constitute the
13 lamellar bodies for more effective access of therapeutic
14 moieties to sequestered micro-organisms protected by
15 prokaryote- and eukaryote-derived linear macromolecules.

16
17 Basic laboratory testing of the effect of lamellar bodies
18 (with the testing being carried out using synthetic
19 lamellar bodies) on the adhesiveness, viscosity and
20 fluidity properties of secretions has, for the first
21 time, shown that the lamellar bodies significantly modify
22 the physical properties of mucus. It has further been
23 shown that synthetic lamellar bodies also have a
24 significant effect on polymeric DNA and actin which can
25 be derived from dead host cells and bacteria. Likewise,
26 synthetic lamellar bodies have been shown to modify
27 physical properties, including viscosity and adhesiveness
28 of alginate of the type secreted by pathogens responsible
29 for a range of life-threatening disorders.

30
31 **Physical and biological properties of mucous secretions**

32 Mucus is the archetypal slimy substance, which coats many
33 epithelial surfaces and is secreted into fluids, such as

1 airway surface fluid, saliva and gastro-intestinal
2 juices. Mucus forms a layer adherent to epithelial
3 surfaces of the respiratory, alimentary and genito-
4 urinary tracts. There it acts to entrap micro-organisms,
5 to provide a diffusion barrier against contact with
6 noxious substances (e.g. inhaled smoke, gastric acid) and
7 allegedly to serve as a lubricant to minimise shear
8 stress damage to the delicate membranes.

9
10 Mucus is composed of polymeric glycoproteins suspended in
11 water that contains electrolytes. It has an extended
12 polypeptide backbone (apomucin), with numerous
13 oligosaccharide side chains. Covered by abundant
14 polyanionic charges, mucus, on exocytotic release from
15 goblet cells, becomes extensively hydrated. Resistant to
16 dehydration, it possesses unique rheological properties
17 of high elasticity, adhesiveness and low solubility.
18 Mucin monomers are polymerized through end-to-end
19 disulphide bonds to form linear polymers which in
20 respiratory mucus are at least 30μ long. Mucus forms a
21 gel whose three-dimensional structure comprises a tangled
22 network of linear mucin polymers devoid of intermolecular
23 cross bridges. In airway surface liquid in normal
24 individuals, mucin concentration is 1% by weight. In
25 cystic fibrosis, an inherited respiratory disorder, mucin
26 concentration is 3-4%.

27
28 Widespread throughout the animal kingdom, the secretion
29 of mucus from body surfaces, in association with
30 underlying motile projections of cell surfaces, cilia,
31 together constitutes an important mechanical system for
32 automatic clearance of potentially noxious substances.
33 In lung, the mucociliary clearance system is the first

1 line of defence against inhaled particulates, aerosols
2 and pathogens, into its airways. Such materials are
3 adsorbed out of the air stream onto the mucous gel
4 contained within the airway surface liquid that coats the
5 ciliated epithelium. The focus of intensive research in
6 recent years, particularly in relation to pathogenesis of
7 cystic fibrosis, there remain unsolved biophysical
8 problems understanding the function of mucociliary
9 clearance in all body surfaces.

10
11 Research work on mucus carried out by the inventor has
12 revealed totally new insights into the functioning of
13 mucus throughout the body. Data provided by these
14 studies supports the hypothesis that where the
15 mucociliary system is present it is invariably
16 accompanied by an integrated parallel system whose
17 secretory product modifies and controls the physico-
18 chemical, and biological properties of mucus. Through
19 the unmasking of the hitherto unrecognized nature and
20 importance of respiratory serous secretions as an
21 essential part of the lamellar body secretory system,
22 satisfactory explanations for anomalous observations and
23 unsolved problems of the physics, molecular biology and
24 pathophysiology of mucociliary clearance have been found.

25
26 Until now, mucous secretion has been viewed as a
27 coherent, self-contained secretory system whose principal
28 function is to provide a substance, which serves as the
29 major protectant of epithelial surfaces throughout the
30 body. Although recent research has demonstrated that the
31 secretion of mucus by goblet cells is responsive to a
32 very wide range of factors from organismal products,
33 through cytokines to neural and hormonal stimuli, there

1 has been no appreciation that a parallel system of
2 secretory cells releases microbodies onto epithelial
3 surfaces which have a profound modifying effect on the
4 consistency, properties and disposal of mucus. This is
5 the much neglected and poorly understood secretion of the
6 serous cells that are always found in association with
7 goblet cells.

8
9 It has long been recognized that throughout respiratory
10 airways there were two cell populations in the surface
11 epithelium, the predominant type being mucous secreting
12 cells called goblet cells and the lesser known serous
13 secreting. Whereas goblet cells release a thick or
14 viscous secretion, serous cells were credited with the
15 production of a thin watery solution. Mucous secretion
16 has received by far the most attention from biological
17 researchers, in comparison to the serous cells whose
18 secretion has been largely ignored. The reason for the
19 disregard lies in the unfortunate failure to identify
20 accurately the nature of the secretion. This was due to
21 the fact that tissue from the respiratory passages, fixed
22 and processed using standard techniques for examination
23 by electron microscopy, did not preserve the contents of
24 the secretory vesicles within the serous cells which
25 appeared to be empty. When however, the cells were fixed
26 with tannic acid and glutaraldehyde, the vesicles are
27 shown to contain osmiophilic phospholipid bilayers
28 arranged in complex geometric patterns. These are
29 lamellar bodies.

30
31 Of the few investigations carried out on serous cells, it
32 was observed that those in the respiratory tree,
33 sometimes called Clara cells, did produce phospholipid

1 microbodies. However, the possibility that airways
2 surface fluid contained a balanced mixture of thick,
3 visco-elastic polymer and a highly efficient lubricant
4 microbody has not been considered by research workers in
5 this field. Indeed, the inventor has demonstrated that
6 this dual partnership of mucus and lamellar bodies
7 locally produces a combined and balanced solution with
8 two ingredients with opposing physico-chemical
9 properties. The body surfaces in the respiratory,
10 gastro-intestinal and genito-urinary tract contain cells
11 that secrete mucus and cells that secrete lamellar
12 bodies. The relative proportions of each type of cell
13 varies from site to site according to the proximity to
14 major, local changes in anatomy, e.g. sphincters, and in
15 time and rate of secretion in response to physiological
16 or pathological stimuli.

17
18 In conclusion, the recent discoveries of the inventor,
19 using electron microscopy, of the ubiquity of lamellar
20 body secreting cells and especially the demonstration
21 that they are found in tandem with mucous secreting
22 cells, has provided new insights into the existence of a
23 balanced system which exercises control over the micro-
24 environment of surfaces and ducts. As predicted by
25 ultrastructural research on this recently discovered
26 secretory system, the creation of synthetic lamellar
27 bodies has provided for the first time in vitro
28 confirmation of the modifying effect of lamellar bodies
29 on the physical properties of secretions and exudates
30 containing linear macromolecules.

31
32 **DNA, actin and alginate in pathological secretions and**
33 **exudates**

1 All of these substances are recognized as viscous
2 molecules released in considerable amounts in a range of
3 pathological processes, principally but not exclusively
4 associated with organismal-induced inflammation. They may
5 be involved usually with mucus, individually or in
6 concert, in a conglomerate thickening of secretions or
7 exudates in a variety of disorders, resulting in serious
8 organ and tissue dysfunction through blockage of ducts
9 and passages, including the Eustachian tube and middle
10 ear in chronic otitis media, and in forming impenetrable
11 layers on working surfaces.

12
13 There would appear to be a provision throughout the
14 animal kingdom for the modification of the physical
15 properties of these linear biological macromolecules.

16 17 **DNA and actin**

18 DNA released from the nuclei of dead cells forms an
19 extremely sticky substance. At a concentration of only
20 1%, polymeric DNA forms a solid gel in vitro. The volume
21 of DNA released from dead leucocytes in an inflammatory
22 process is considerable. Thus, sputum in cystic fibrosis
23 may contain up to 10% DNA by weight. The linear
24 macromolecule actin, principal constituent of the
25 filamentous cytoskeleton, constitutes 20% of the total
26 protein present in the average cell. This substance,
27 likewise, is a viscous molecule which is released in
28 significant amounts by dead leucocytes, further adding to
29 the viscosity of inflammatory secretions and exudates.
30 Additionally, both DNA and actin are released in not
31 inconsiderable amounts from dead bacteria when present in
32 infective processes.

1 Bacterial-derived alginate

2 The bacterium, *Pseudomonas aeruginosa*, causes serious
3 chronic infections throughout the body, including chronic
4 otitis media, chronic sinusitis, and especially in the
5 respiratory tract in patients with cystic fibrosis.
6 Mucoid colonies of these organisms secrete an
7 extracellular polymeric substance (EPS) known as
8 exopolysaccharide alginate which significantly enhances
9 their pathogenicity. The alginate is a straight-chain,
10 hydrophilic, colloidal, polyuronic acid composed
11 primarily of anhydro-beta-D mannuronic acid residues with
12 1-4 linkage. A viscous linear macromolecule, this
13 alginate not only contributes significantly to the
14 thickening of secretions colonized by the bacteria, but
15 forms a biofilm which protects it from phagocytosis by
16 macrophages.

17

18 These linear macromolecules constitute a serious hazard
19 to drainage and clearance of secretions and exudates.

20

**21 Surgical procedures where mucus, DNA, actin and alginate
22 are a problem**

23 In many disease states the overproduction of mucus often
24 occurs and is particularly problematic when surgical
25 procedures are to be carried out. In most sites and
26 conditions the overproduction of mucus is accompanied by
27 pathological production and release of linear
28 macromolecules (DNA, actin, alginate). Even in cases
29 where mucus production is normal it can still be
30 obstructive in surgical procedures.

31

32 Functional Endoscopic Sinus Surgery (FESS)

1 FESS is a minimally invasive procedure for the treatment
2 of chronic sinusitis. It is designed to remove blockage
3 and provide free drainage of the sinus. FESS causes
4 little tissue damage and there is no visible scarring
5 that is associated with open surgery. FESS is often
6 recommended in cases of chronic sinusitis that do not
7 respond well to medication or other forms of treatment.
8 This occurs when the sinuses are blocked and unable to
9 drain the mucus. When this happens, the sinuses can
10 become infected.

11
12 The FESS procedure uses an endoscope, which enables the
13 surgeon to identify and correct anatomic causes of sinus
14 outflow obstruction. Other surgical instruments may be
15 inserted alongside the endoscope to treat problems inside
16 the sinuses. The kind of surgery will depend on the
17 extent of the sinus problem. Sometimes other nasal
18 procedures may be performed with the sinus surgery to
19 improve access and drainage of the sinuses. In the
20 present case we are suggesting that lamellar bodies or
21 synthetic lamellar bodies can be used to modify the mucus
22 prior to or during the procedure.

23
24 Typically the procedure will include the steps of:

- 25 • applying a composition including lamellar bodies to
26 the sinus
- 27 • allowing the lamellar bodies in the composition to
28 modify the viscosity of the mucus and any admixed
29 linear macromolecules such as DNA, actin or alginate
30 in the area of the sinus such that it is capable of
31 being removed
- 32 • introducing a surgical instrument to the nasal
33 passage such as to remove tissues from the sinus

1

2 The amount of lamellar bodies in the composition is
3 variable but typically the dosage concentration of
4 lamellar bodies in the composition will be 10×10^9 per
5 ml. The composition can take the form of a spray
6 (nebulized, with and without ultrasonification), an
7 injection or a slow-release preparation.

8

9 **Other surgical areas**

10 As well as being useful in ear, nose and throat
11 procedures such as FESS and surgical treatment of Otitis
12 Media, lamellar bodies can also be used in tract and
13 ductal surgery where the secretion of mucus with or
14 without admixtures of linear macromolecules such as DNA,
15 actin and alginate, can make the procedure more
16 difficult. Most commonly this will be applicable in
17 surgery of the hepato-biliary ducts and gall bladder,
18 pancreatic surgery, liver surgery, tracheal surgery,
19 reproductive tract surgery, surgery of the salivary and
20 lachrymal glands, including flushing of ducts, and
21 surgery or descaling of the gastro-intestinal tract (in
22 the cases the term surgery relates to procedures that
23 will typically be carried out by a surgeon).

24

25 **Fistula and pathological sinuses**

26 "Fistula" is a term which describes the formation of an
27 abnormal passageway which develops due to a pathological
28 process. A fistula is usually a narrow tube lined not
29 with an epithelial surface but with granulation tissue
30 which connects two body surfaces, either between two
31 hollow viscera or between a hollow viscera and a body
32 surface. Examples of this are a fistula which develops
33 between colon and urinary bladder (vesico-colic fistula),

1 and vagina and colon (vagino-colic fistula). Such lesions
2 are notoriously difficult to eradicate and give rise to
3 persistent focal, chronic and acute-on-chronic
4 inflammation. Intermittent blockage and/or loculation of
5 the fistula's lumen by thickened secretions of varying
6 admixtures of mucus, DNA, actin and alginate are the key
7 players in its maintenance and create serious obstacles
8 to its surgical removal and closure. Instillation of
9 topical antibiotics has minimal effect, due to blockage
10 and coating of the fistula wall by thickened,
11 impenetrable secretions. What is currently unavailable to
12 surgeons is a biologically effective substance which will
13 cleanse the fistula of the secretions harbouring
14 bacteria, endotoxin, pro-inflammatory cytokines and
15 provide a period of continuous drainage to allow
16 suppression of the inflammation in the wall of the
17 fistula and clearance of pathogenic bacteria to permit
18 successful surgical excision of the fistula's tract.
19 Fistula are typically encountered in chronic inflammatory
20 bowel disorders, including Crohn's disease and ulcerative
21 colitis.

22
23 In the present case it is suggested that lamellar bodies
24 or synthetic lamellar bodies can be used as a preparatory
25 treatment as an adjunct for successful surgical treatment
26 or eradication of pathological sinuses and fistulae.
27 Typically, the procedure will include endoscopy of the
28 affected viscera or organ to gain access for inserting a
29 catheter into the sinus tract for applying a composition,
30 including lamellar bodies, thereby introducing a flushing
31 solution containing lamellar bodies or introduction of
32 slow-release matrices, enteric-coated or biodegradable
33 capsules containing lamellar bodies.

Other treatment areas where modification of mucus is therapeutic

In a wide range of disorders, secretions may become so thickened that, rather than protecting surfaces or ducts, their viscosity causes severe local functional derangement. The pathophysiology responsible for the alteration in physical properties of the secretions is only partially understood. A prime cause of thickened mucous secretion is stimulation by endotoxins and cytokines, resulting in a proliferation of cells that secrete mucus. It is also recognized that the degree of hydration of mucus has a significant effect on its viscosity (particularly in cases such as cystic fibrosis).

Radiation-induced mucositis

Following radiation therapy of the head and neck, areas of the nasopharynx, pharynx, larynx and trachea may exhibit a troublesome inflammation of the epithelial surfaces, resulting in thick exudates and secretions. These viscous, adhesive membranes harbour bacteria, endotoxins and pro-inflammatory cytokines which promote and prolong chronic inflammation at these sites, preventing healing. There is provided a method for applying a composition including lamellar bodies in a variety of forms including aerosol spray with or without ultrasonification, a suspension or gel to the areas affected by mucositis for the dispersement of the adhesive membrane, promoting healing of the inflamed areas.

1 Sinusitis

2 Sinuses are membrane-lined openings in the bones around
3 the nose. Four pairs of sinuses are connected to the
4 nasal cavity by small openings and these sinus cavities
5 rest alongside the nose, above the eyebrows and behind
6 the cheekbones.

7

8 Normally, air passes in and out of the sinuses and mucus
9 drains from the sinuses into the nose. When there is an
10 obstruction, fluid is unable to pass through the sinuses
11 freely. When sinuses are infected, membranes become
12 swollen as blood rushes to the infected area. This
13 swelling causes congestion, facial pain and increased
14 mucus production. As a result, the nose may become runny
15 and drippy. The mucous secretions may thicken over time
16 creating a breeding ground for infections.

17

18 Acute sinusitis typically follows a cold and lasts for a
19 few weeks. In the case of chronic sinusitis, the
20 sinusitis may recur a number of times over the year.
21 Typically, antibiotics and decongestants are used to
22 treat the condition, although in the case of chronic
23 sinusitis additional treatment methods are also often
24 used.

25

26 In the present invention, it is suggested that a
27 composition containing lamellar bodies can be used to
28 treat sinusitis. The composition could take any form but
29 typically would be in the form of a spray or nebulized
30 formulation. As lamellar bodies modulate the viscosity
31 of mucus this would help to relieve the symptoms of
32 sinusitis. It can also be seen that a similar or the
33 same formulation could be used to treat symptoms of the

1 common cold or influenza. This would be particularly
2 useful in the form of a nasal spray.

4 **Cystic Fibrosis**

5 Cystic fibrosis (CF) is the most common, lethal,
6 autosomal recessive disorder in people of European
7 extraction, affecting one in four thousand infants born
8 per annum in the United States and Canada. Patients with
9 CF die at an early age of respiratory failure due to
10 profound lung injury secondary to colonization by
11 pathogens and chronic inflammation of pulmonary tissues.
12 The median survival age in North America for patients
13 with CF had by 1996 reached thirty, whereas in South
14 America it was nine years. Thus socio-economic conditions
15 and availability of resources determine whether or not
16 patients receive optimal care. These factors play an
17 important role in the morbidity and longevity of
18 individuals with this disorder.

19
20 The genetics of CF are now relatively well-understood. As
21 an autosomal recessive disorder, both parents of an
22 affected infant must carry the gene, and each pregnancy
23 carries a one in four chance of producing a child with
24 CF. The carrier rate in Europeans and their descendants
25 is about one in twenty-eight, with the rate in other
26 ethnic groups generally being lower. In 1989 the gene
27 responsible for CF was located on the long arm of
28 chromosome 7. Mutations cause either deficiency or
29 absence of a membrane-spanning glycoprotein responsible
30 for the maintenance of the ion channel which allows
31 efflux of anions through the cell membrane in epithelium
32 throughout the body. The protein is called the Cystic
33 Fibrosis Transmembrane Conductance Regulator (CFTR). This

1 channel renders the cell membrane permeant to chloride
2 and other larger organic anions such as reduced
3 glutathione (GSH). Despite this knowledge, there is
4 however, a missing linkage between the genetics and the
5 resultant pathology in CF.

6
7 The CFTR gene is found in epithelial cells of the
8 respiratory, intestinal, hepato-biliary and reproductive
9 tracts. It is also found in exocrine glands such as the
10 serous glands in lung and in pancreas. Absence or
11 dysfunction of the CFTR protein results in thick,
12 viscous, mucous secretions in sinuses, lungs, biliary
13 cannaliculae, intestines and epididymis, resulting in
14 bronchiectasis, chronic liver disease, biliary and
15 intestinal obstructions, infertility, pancreatic
16 insufficiency and diabetes.

17
18 The essential pathological features of CF can be
19 explained through blockage by viscous secretions of the
20 cannaliculae, ducts and passages in tissues and organs
21 where the lining epithelia are affected by the genetic
22 deficiency. This results in progressive cyst formation,
23 chronic inflammation and infection which weakens then
24 destroys the walls of the ducts and passages, typically
25 as encountered in bronchiectasis and pulmonary fibrosis,
26 which are responsible for the greatest threat to life.
27 Nevertheless, current research acknowledges the existence
28 of a missing linkage between the genetics, its molecular
29 expression and the pathogenesis of the lesions in the
30 different tissues which characterises CF as a defined
31 disorder.

1 When it was discovered that the CF gene was responsible
2 for the CFTR protein which controlled a chloride channel,
3 its role in controlling the volume and electrolyte
4 composition of sweat was established. Thus it was
5 naturally assumed that a similar dysfunction in lung
6 could explain the increased viscosity of the mucus via
7 the hypothesis of abnormal salt concentration and low
8 volume of airway surface fluid. Unfortunately, most
9 evidence to date indicates that airway surface fluid is
10 isotonic and of normal volume. Since electrolytes
11 together with colloids are the key determinants of water
12 distribution in tissue spaces, it was realised that the
13 effect of the CFTR protein must be responsible for
14 deficiencies other than electrolytes in the micro-
15 environment within ducts and on surrounding epithelial
16 surfaces. Therefore, in a continuing search for a
17 molecular linkage between the gene defect and the
18 resultant pathology, deficiencies of other anions have
19 been sought. Of these, the ubiquitous tripeptide, reduced
20 glutathione (GSH), one of the body's most important
21 water-soluble anti-oxidants, has been considered a
22 candidate for the missing linkage. GSH is present in
23 extracellular epithelial fluids such as the airway
24 surface fluid, gastro-intestinal juices, semen, etc. In
25 the extracellular milieu, GSH provides powerful anti-
26 oxidant protection to surfaces heavily exposed to
27 reactive oxygen species, as in the lung airways where its
28 concentration is 140 times the normal level in blood
29 plasma. However, despite these actions of GSH, most
30 workers in the field are of the opinion that they provide
31 only a partial explanation for the resultant pathology.

1 In conclusion it is openly acknowledged by research
2 workers that the true nature of the pathophysiology of CF
3 is unknown and that the search should be extended for a
4 missing factor or factors.

5
6 There is no single therapeutic procedure which
7 successfully prevents the ultimate progression of the
8 pathologies which result in death. The major effort in
9 the treatment of CF is devoted to combating broncho-
10 pneumonitis. The objective is to minimise tissue damage
11 by facilitating bronchial clearance of viscous, infected
12 mucus (chest physiotherapy, broncho-dilators,
13 mucolytics), and reducing bacterial burden (antibiotics).

14
15 Although the pathophysiology is not yet understood,
16 viscous mucus in CF lungs is acknowledged as being a
17 major factor in the pathogenesis of the lesions.
18 Recently, it has been realised that DNA, actin and P.
19 aeruginosa-derived alginate play a significant
20 aggravating role in thickening secretions and exudates in
21 CF. There is thus an ongoing strategy to investigate the
22 role of such substances in pathological secretions in CF
23 and thereby to develop agents based on this premise to
24 alleviate some of the features of airway obstruction.

25
26 The first product to reach the marketplace as a result of
27 this strategy is recombinant human DNase (rhDNase). It is
28 well-established that infected secretions in CF lungs
29 contain as much as 10% DNA as a result of the continual
30 breakdown of bacteria and neutrophils in chronically
31 infected lungs. Extracellular DNA forms long molecular
32 chains which increase the visco-elasticity of the
33 secretions. RhDNase alters the physical properties of CF

1 secretions both in vitro and in vivo. Currently, some 50%
2 of CF patients in the USA receive rhDNase and it has been
3 demonstrated that patients cough less and have less thick
4 sputum. Its impact on lung function, however, is small.
5 Young patients with mild lung disease given a six months
6 course of rhDNase produced only a 3% benefit in FEVI, but
7 it decreased the frequency of intravenous antibiotic
8 courses by 34%.

9
10 Another compound believed to have the potential to
11 decrease sputum viscosity is gelosin, which breaks down
12 polymeric filamentous actin (F-actin), another component
13 in the thick secretions which makes an important
14 contribution to its viscosity. Although polymeric F-actin
15 makes up around 10% of CF sputum, clinical studies on the
16 efficacy of gelosin have to date been disappointing.

17
18 With respect to patient tolerance of both agents, studies
19 have shown that gelosin and DNase may activate
20 inflammatory mediators such as Interleukin 8, and may
21 explain the disappointing impact of these compounds on
22 lung function.

23
24 A further new approach to thinning thickened secretion in
25 CF patients is the use of low-dose macrolide antibiotics,
26 which interferes with the ability of pseudomonads to
27 manufacture alginate, a major component of the protective
28 coating of these bacteria. When these bacteria reach a
29 critical density, they produce large quantities of
30 alginate, creating a biofilm which interferes with the
31 penetrance of antibiotics, access of acute inflammatory
32 cells to the bacteria and hinders the clearance of the
33 thickened secretions from airways in CF patients.

1
2 Separate products have therefore been individually
3 developed with a view to facilitating the clearance of
4 mucus, DNA, actin and bacterial-derived alginate in the
5 grossly thickened secretions in CF patients with only
6 relative success.

7
8 In the knowledge that lamellar bodies are secreted by
9 serous cells in the airways, and in light of the fact
10 that it has been shown by Applicant that lamellar body
11 secretion in extrapulmonary sites is responsible for
12 lubrication of serous cavities throughout the animal
13 kingdom, ex vivo investigation of the effect of synthetic
14 lamellar bodies on mucus, DNA, actin and bacterial-
15 derived alginate was carried out. As demonstrated herein,
16 the results confirmed that synthetic lamellar bodies
17 significantly decrease the viscosity of mucus, polymeric
18 DNA, actin and alginate in vitro studies.

19
20 Therefore synthetic lamellar bodies possess the ability,
21 as shown in vitro, to alter the viscosity, adhesiveness
22 and fluidity of the individual and combined components of
23 the thickened secretion in CF patients, in contrast to
24 current therapeutic endeavours which have been directed
25 at formulating specific agents for each component
26 involved in the pathological process.

27
28 Accordingly, the inventor maintains that CF may be
29 treated by exposure of the composite, pathologically
30 thickened secretions to synthetic lamellar bodies. This
31 will be achieved by restoration of adequate local levels
32 of lamellar bodies, sufficient for the diminution of

1 viscosity and adhesiveness, while increasing the fluidity
2 and clearance of pathological secretions.

3

4 Furthermore, the inventor maintains that in CF a key
5 factor in the pathogenesis of the disorder is relative
6 failure of the lamellar body system to secrete adequate
7 volumes of phospholipid microbodies to balance the
8 physical properties of mucus and the pathological debris
9 produced by intercurrent local inflammation (DNA, actin
10 and alginate). Thus therapeutic effect is achieved by
11 regular intermittent application of lamellar bodies to
12 the affected tubal systems and surfaces, where the
13 lubricating microbodies, as has been demonstrated in
14 vitro, penetrate with ease the interstices of the gel-
15 like structure of the thickened secretions.

16

17 **Other Disease States**

18 There are a number of other disease states in which
19 linear macromolecules are central to their pathogenesis
20 and progression of the condition in a manner outlined in
21 detail in cystic fibrosis, where lamellar bodies or a
22 lamellar body composition could be used to beneficial
23 effect. These include respiratory disorders such as
24 bronchitis and chronic bronchitis, asthma, bronchiectasis
25 and chronic obstructive pulmonary disease. Additionally,
26 disorders affecting the gastro-intestinal, hepato-
27 biliary, pancreatic and reproductive tracts are subject
28 to organismal and auto-immune induced thickened
29 secretions. A variety of wounds affecting skin, such as
30 thermal and radiation burns, chronic ulcers and de-
31 gloving injuries with extensive loss of epidermis, dermis
32 and full thickness skin, share a common pathological
33 feature of adhesive and viscous exudates. Likewise, these

1 constitute conditions where lamellar bodies or a lamellar
2 body composition, could be used to beneficial effect.

3

4 The Skin: Lamellar Bodies in the Treatment of Thermal
5 and Radiation Burns, in Chronic Ulcers and in Wounding
6 Involving Extensive Loss of Epidermis, Dermis and Full
7 Thickness Skin

8 In burning injuries to skin, areas of loss of epidermis
9 and dermis, down to full thickness skin, present a raw
10 wound which is typically covered by viscous, highly
11 adhesive exudates consisting of DNA and actin released
12 from the nuclei of host-derived dead epidermal and dermal
13 cells, leucocytes and pus cells, together with DNA and
14 actin released from dead colonising bacteria. The
15 viscosity and adhesiveness of the exudates in many
16 instances are further increased with the onset of
17 significant infection by alginate-secreting organisms
18 such as *Pseudomonas aeruginosa*, a frequent and
19 troublesome infection in burns injuries.

20

21 The viscous and adhesive properties of the burns exudates
22 give rise to several key pathological effects which
23 seriously compromise wound healing. The most damaging
24 effect of the exudates is its tenacious adherence to
25 wound dressings of all types and textures. Each time
26 dressings are removed, the wound surface is traumatised,
27 resulting in an out-pouring of fresh fibrin. This not
28 only causes the patient extreme pain but also, this
29 regularly repeated insult creates stratified layers of
30 dense fibrin which seriously retard the healing process
31 and are pathogenetically responsible for over-production
32 of collagen and consequent scarification and deformity.

33

1 The viscous and adhesive burns exudate also impedes and
2 restricts the ingress and movement of cells essential for
3 the scavenging of debris, the phagocytosis of bacteria
4 and cells involved in structural repair and re-
5 epithelialisation.

6

7 The viscous exudates, DNA and actin, provide sanctuary
8 areas which foster infection, while colonisation by
9 organisms which actively secrete biofilm (alginate) then
10 further augment the pathological effect of viscosity and
11 adhesiveness. This sequential process progressively
12 shields the colonising organisms from attack by
13 phagocytic cells and seriously restricts the penetration
14 of antibiotics into the constantly thickening exudate.

15

16 It should be noted that lamellar bodies are normally
17 produced in human skin by the keratinocytes. We have
18 shown that in cell culture, replicating immature human
19 keratinocytes vigorously secrete lamellar bodies.
20 Although the scientific community has not yet considered
21 the role of lamellar bodies in the promotion of wound
22 healing, our detection by electron microscopy of their
23 presence in skin and peritoneal wounds, strongly
24 indicates the appropriateness of topical administration
25 of lamellar bodies to wounds, particularly in burns,
26 where the pathological presence of viscous and adhesive
27 linear macromolecules seriously compromises healing and
28 repair.

29

30 **Chronic Skin Ulcers**

31 A diverse range of chronic ulcers are encountered in
32 skin. This occurs most commonly in lower limb and foot,
33 particularly in diabetes mellitus, venous stasis and

1 peripheral vascular disease. As with burns injuries,
2 viscous and adhesive exudates consisting of DNA, actin
3 and bacterial-derived alginates when present as a film on
4 the surface of the ulcer base can seriously impair wound
5 healing. This is a major factor in the maintenance of
6 chronicity in ulcers of this type. As in the standard
7 treatment of burns, adhesion of occlusive dressings to
8 the ulcer base results in continual micro-trauma to the
9 delicate membrane each time they are removed. This
10 process therefore causes repeated episodic oozing of
11 fresh fibrin over the base of the ulcer. Since fibrin is
12 the major stimulus to production of granulation tissue,
13 frequent episodes of fibrin exudation create a permanent
14 state of early-stage wound repair in the base of the
15 ulcer which effectively blocks the natural progression to
16 resolution and re-epithelialisation.

17
18 **Wounding Involving Extensive Denudation of Epidermis,**
19 **Dermis Down to Full Thickness Skin (De-gloving Injury)**

20 Loss of skin in injuries of this nature creates a form of
21 wound not dissimilar to that caused by burning. Likewise,
22 occlusive dressings adhere tenaciously to the range of
23 viscous molecules present in the surface exudate.
24 Frequent or daily stripping of occlusive bandages
25 provokes episodic exudation of fibrin, resulting in
26 similar pathological sequelae encountered in burns and
27 chronic ulcers.

28
29 **Methods of Therapeutic Application**

30 The following methods are applicable for diverse types of
31 wounds, burns, chronic ulcers, de-gloving injuries.
32 Wounds are sprayed with a suspension of lamellar bodies
33 or a lamellar body composition before the dressings are

1 applied. Preferably dressings should have micro-
2 perforations of a diameter sufficient to allow passage of
3 lamellar bodies through into the underlying wound.
4 Likewise, the density of the pores per unit area shall be
5 appropriate to adequate delivery of lamellar bodies to
6 the underlying interface between the dressing and the
7 wound when a suspension of lamellar bodies are sprayed
8 over the outer surface of the dressing .The perforations
9 on the dressings preferably should be of a density which
10 does not compromise the occlusive properties of the
11 dressing with respect to ingress of bacteria. At an
12 appropriate time interval before its removal, dependent
13 on the rate of delivery of lamellar bodies to the wound
14 surface, the dressing will be sprayed with a suspension
15 of lamellar bodies which passes through the perforations
16 into the space between it and the wound surface.

18 **Dressings Incorporating Lamellar Bodies**

19 A further method of application is the provision of
20 dressings incorporating lamellar bodies which are
21 released gradually from the under surface of the dressing
22 onto the wound surface. This may be achieved by their
23 containment in a thin envelope within the dressing which
24 acts as a reservoir for slow release of lamellar bodies
25 through microscopic perforations by incorporating a
26 porous membrane on the inner surface.

28 Lamellar bodies may also be incorporated in a dressing
29 whose under surface is coated with a matrix or a gel from
30 which they are released. Biocompatible gels would include
31 hyaluronan and/or chondroitin sulphate. These gels are of
32 lower viscosity compared to the pathological exudates
33 present in wounds against which the lamellar bodies are

1 directed, and the presence of lamellar bodies would
2 confer a fluid, non-stick surface at the interface
3 between wound and dressing.
4

5 **Use of Lamellar Bodies in Disorders of the Mucous**
6 **Membranes (Mucositis)**

7 Inflammation of mucous surfaces, particularly those close
8 to the body openings (buccal cavity, oropharynx, larynx,
9 male and female genito-urinary tracts, and anal canal)
10 are subject to painful inflammation, erosion and
11 ulceration. A generic term, mucositis, denotes a not
12 uncommon affliction caused by a wide spectrum of
13 aetiological factors, ranging from radiation,
14 chemotherapeutic agents, drugs, auto-immunity , to
15 allergies and infections. A characteristic feature of
16 these conditions is the dryness of the surfaces which
17 become covered with sticky exudates consisting of viscous
18 mucus, viscous DNA and actin from dead cells and
19 bacteria. In extreme cases, opposing surfaces adhere one
20 to the other forming synechiae, as in the oropharynx,
21 prepuce, labia and vagina. Swallowing or slight movements
22 affecting the surfaces are very painful. Separation of
23 opposing surfaces causes repeated micro-trauma to the
24 mucous membrane such as to promote ulceration and prevent
25 healing. Specific dermatological disorders which give
26 rise to these problems include Stevens-Johnson syndrome,
27 Pemphigus, Behcet's disease, systemic lupus erythematosus
28 and other bullous disorders. A suspension of lamellar
29 bodies in physiological saline applied by regular
30 spraying of the affected areas, or the application of
31 lamellar body-containing gels or matrices will restore
32 lubricity and non-stick properties to the dry, adherent
33 surfaces. Application of lamellar bodies to affected

1 mucous surfaces will decrease viscosity of the
2 pathological secretions and exudates, solubilised
3 crusting and prevent formation of synechiae.
4

5 **Use of Lamellar Bodies in Inflammatory Conditions of the** 6 **Eye**

7 Lamellar bodies are found in tears. We have shown by
8 immunocytochemistry using the monoclonal antibody that
9 the lacrimal epithelia stain positively for surfactant
10 protein A. This indicates that lamellar body secretion is
11 a constitutive function of lacrimal glands in man. The
12 mucous membrane of the eyelids and the conjunctivae are
13 normally moistened by a thin fluid. In pathological
14 conditions the external surfaces of the eye may become
15 dry and/or covered by thickened viscous secretions or
16 exudates. These exudates may form crusts whose abrasive
17 effect further excoriates and traumatises the inflamed
18 surfaces. A wide variety of disorders give rise to
19 lesions of this nature. In the common autoimmune
20 disorders, rheumatoid and Sjogren's syndrome, an
21 irritating dryness of the eyes called kerato-
22 conjunctivitis sicca is a frequent occurrence. A wide
23 variety of other disorders, inflammatory disorders due to
24 viral or bacterial infection, allergies, adverse drug
25 reactions give rise to blepharitis and conjunctivitis
26 with accompanying viscous secretions and exudates.
27 Regular administration of suspensions of lamellar bodies
28 as eyedrops would be an appropriate therapeutic strategy
29 whose usefulness and biocompatibility would be ascribed
30 to the restorative effect of natural tears. Lamellar
31 bodies may also be applied in the form of gel, matrices
32 or slow-release devices or excipients.
33

1 **Production of synthetic lamellar bodies**

2 The focus of the present invention is the therapeutic use
3 of lamellar bodies. The following information provides
4 details of their production and the key features and
5 composition, which characterises them as a novel
6 microbody. In contrast to liposomes, whose invention from
7 the outset was not based on a concept in any way related
8 to a naturally-occurring microbody, synthetic lamellar
9 bodies are designed to mimic a range of biological
10 activities ascribed to naturally-occurring lamellar
11 bodies in tissues and body cavities. The principal
12 differentiating characteristics of naturally-occurring
13 lamellar bodies are:

- 14 1) On contact, lamellar bodies, both divide easily and
15 fuse readily one with the other in body cavities and
16 tissues when subjected to movement and shear stress.
17 2) The provision of lubricity.
18 3) The automatic surface adsorption of planktonic
19 molecular debris arising from inflammatory
20 processes, etc.
21 4) The automatic, non-receptor-mediated endocytosis of
22 lamellar bodies by the monocyte/phagocyte system,
23 (and most especially by antigen presenting cells,
24 dendritic cells and macrophages).

25

26 These properties are crucially dependent on the nature of
27 the mix of the different species of phospholipids
28 (phosphatidylcholine, sphingomyelin,
29 phosphatidylethanolamine, phosphatidylserine and
30 phosphatidylinositol) and the nature of their fatty acid
31 chains whose heterogenicity, length and range of
32 saturation and unsaturation leading to lamellar fluidity

1 is of key importance for their striking range of
2 biological activities.

3
4 In contrast to lamellar bodies, liposomes must on no
5 account split or fuse. This is achieved by their
6 different composition, conferring a necessary rigidity
7 through high proportions of cholesterol and use of more
8 rigid phospholipids which, together greatly reduces
9 membrane fluidity. Liposomes are not designed to confer
10 lubricity. The composition of liposomes is chosen not to
11 confer any surface adsorptive properties, a feature which
12 would be totally incompatible with liposomal usages.
13 Liposomes are specifically designed not to be
14 phagocytosed by the monocyte/phagocyte system, which
15 would preclude any form of organ- targeted drug delivery
16 which has been their prime, relatively unsuccessful use.
17 Hence the development of Stealth liposomes in an attempt
18 to obviate the biologically incompatible inherent paradox
19 in the current formulation of liposomes.

20
21 The principal phospholipid constituents of lamellar
22 bodies are phosphatidylcholine (PC), sphingomyelin (SPH),
23 phosphatidylethanolamine (PE), phosphatidylserine (PS),
24 phosphatidylinositol (PI) and lysolecithin (LPC). The
25 phospholipid composition of lamellar bodies shows slight
26 variation according to the cell of origin.

27
28 PC is the principal phospholipid in lamellar bodies,
29 irrespective of site of origin. The percentage PC
30 concentration varies from around 70% in lung lavage to
31 45% in synovial fluid (Refs). The next phospholipid in
32 ranking concentration is SPH (15-23%). Thereafter, PE,
33 PS, PI, PG and LPC are present in varying, single digit

1 percentage concentrations in lamellar bodies according to
2 site of origin.

3

4 The preferred composition of phospholipids and
5 cholesterol for phospholipid multilamellar microbodies
6 comprises: PC 54%: SPH 19%: PE 8%: PS 4%: PI 3%:
7 cholesterol 10%. These values are median and the
8 following range of compositions have been found in
9 natural lamellar bodies (private research): PC 44-70%,
10 SPH 15-23%, PE 6-10%, PS 2-6%, PI 2-4%, Cholesterol 4-
11 12%. These figures are percentage by weight.

12

13 LPC may also be incorporated into the multilamellar
14 microbodies at 2% by weight which follows the range found
15 in natural lamellar bodies of 0-3%.

16

17 Liposomes are made by those skilled in the art with high
18 cholesterol concentrations to improve their rigidity.
19 Liposomes containing cholesterol at 20% or below would be
20 considered to be cholesterol poor. Thus liposomes
21 incorporating a high ratio (50%) of cholesterol, where it
22 is equimolar with the phospholipids, have a highly stable
23 structure and are the pivotal concept for the creation of
24 liposomes. Until this invention, it would not to our
25 knowledge have been obvious to try using low-cholesterol
26 multilamellar microbodies since the late discovery of
27 lamellar bodies as a ubiquitous biological phenomenon
28 remains unknown and unquoted by anyone working in the
29 liposomal field. The cholesterol content of lamellar
30 bodies derived from pulmonary alveoli has been found to
31 contain around 10% cholesterol.

32

33 The presence of sphingomyelin in natural lamellar bodies

1 and in the synthetic lamellar bodies claimed in the
2 present invention is important. Sphingomyelin is not
3 generally used in liposomes and serves to give
4 flexibility and softness to lamellar bodies.
5 Conventional liposome technology teaches that rigidity is
6 mandatory for the delivery of chemicals; however, we have
7 found that flexible, low-cholesterol, sphingomyelin
8 containing synthetic lamellar bodies are ideal for
9 delivery of antigen to antigen presenting cells and, as
10 demonstrated by vigorous non-receptor mediated
11 endocytosis by dendritic cells of synthetic lamellar
12 bodies, first described by the inventor.

13
14 Phospholipid multi-lamellar microbodies (synthetic
15 lamellar bodies) are prepared by a technique similar to
16 that used to produce hand-shaken multi-lamellar vesicles.
17 The phospholipid mixture, together with cholesterol in
18 the percentages given by weight, is dissolved in a
19 chloroform / methanol solvent mixture (2:1 vol/vol). The
20 lipid solution is introduced into a round-bottomed flask
21 and attached to a rotary evaporator. The flask is
22 evacuated and rotated at 60 r.p.m. in a thermostatically
23 controlled waterbath at a temperature of 30°C until a dry
24 lipid film is deposited. Nitrogen is introduced into the
25 flask and the residual solvent is removed before its
26 connection to a lyophilizer where it is subjected to a
27 high vacuum at room temperature for one hour. After
28 release of the vacuum and following flushing with
29 nitrogen, saline containing solutes (selected antigen)
30 for entrapment is added. The lipid is hydrated within
31 the flask, flushed with nitrogen, attached to the
32 evaporator, and rotated at 60 r.p.m. at room temperature
33 for thirty minutes. The suspension is allowed to stand

1 for two hours at room temperature to complete the
2 swelling process.

3
4 It should be noted that the embodiments disclosed above
5 are merely exemplary of the invention, which may be
6 embodied in many different forms. Therefore, details
7 disclosed herein are not to be interpreted as limiting,
8 but merely as a basis for Claims and for teaching one
9 skilled in the art as to the various uses of the present
10 invention in any appropriate manner.

11

12 **Pharmaceutical Compositions and Methods of Delivery**

13 Another aspect of the invention provides for
14 pharmaceutical compositions comprising purified lamellar
15 bodies for the modification of linear macromolecules.
16 These lamellar bodies may be synthetic or naturally
17 occurring and may act as surrogate lamellar bodies in
18 body cavities, blood vessels, ducts, sinuses and tissues
19 to modify mucus viscosity for therapeutic purposes.

20

21 One embodiment features treatment of a wide range of
22 diseases and conditions with pharmaceutical compositions
23 containing synthetic or naturally occurring lamellar
24 bodies or microbodies and acceptable carriers and
25 excipients. Moreover, a further embodiment may include a
26 pharmaceutical composition designed for use in local
27 treatment of conditions having a preponderance of heavy
28 mucous secretions. Another embodiment may include a
29 pharmaceutical composition designed for systemic use
30 alone or with other standard treatment modalities known
31 to those skilled in the art.

32

1 Such compositions comprise a therapeutically effective
2 amount of an agent, and a pharmaceutically acceptable
3 carrier. In one embodiment, the pharmaceutical
4 composition may be presented in unit dosage forms to
5 facilitate accurate dosing. The term "unit dosage forms"
6 refers to physically discrete units suitable as unitary
7 dosages for human subjects and other mammals, each unit
8 containing a predetermined quantity of active material
9 calculated to produce the desired therapeutic effect, in
10 association with a suitable pharmaceutical excipient.
11 Typical unit dosage forms include prefilled, premeasured
12 ampules or syringes of the liquid compositions or pills,
13 tablets, capsules or the like in the case of solid
14 compositions. The unit can be, for example, a single use
15 vial, a pre-filled syringe, a single transdermal patch
16 and the like. The unit dosage form can be in unit dose or
17 unit-of-use packages. As is known to those skilled in the
18 art, a unit dose package is a convenient, patient ready
19 unit. "A unit dosage form would be a 5ml suspension of
20 lamellar bodies in which there would be 54mg of
21 phosphatidylcholine, 19mg of sphingomyelin, 8mg
22 phosphatidylethanolamine, 4mg phosphatidylserine, 3mg
23 phosphatidylinositol and 10mg cholesterol."
24 In a particular embodiment, the term "pharmaceutically
25 acceptable" means approved by a regulatory agency of the
26 Federal or a state government or listed in the U.S.
27 Pharmacopeia or other generally recognized pharmacopeia
28 for use in animals, and more particularly in humans. The
29 term "carrier" refers to a diluent, adjuvant, excipient,
30 or vehicle with which the therapeutic is administered.
31 Such pharmaceutical carriers can be sterile liquids, such
32 as water and oils, including those of petroleum, animal,
33 vegetable or synthetic origin, such as peanut oil,

1 soybean oil, mineral oil, sesame oil and the like.
2 Sterile isotonic aqueous buffer is a preferred carrier
3 when the pharmaceutical composition is administered
4 intravenously. Saline solutions and aqueous dextrose and
5 glycerol solutions can also be employed as liquid
6 carriers, particularly for injectable solutions.
7 Suitable pharmaceutical excipients include starch,
8 glucose, lactose, sucrose, gelatin, malt, rice, flour,
9 chalk, silica gel, sodium stearate, glycerol
10 monostearate, talc, sodium chloride, dried skim milk,
11 glycerol, propylene, glycol, water, ethanol and the like.
12 The composition, if desired, can also contain minor
13 amounts of wetting or emulsifying agents, or pH buffering
14 agents. These compositions can take the form of
15 solutions, suspensions, emulsion, tablets, pills,
16 capsules, powders, sustained-release formulations and the
17 like. The composition can be formulated as a
18 suppository, with traditional binders and carriers such
19 as triglycerides. Oral formulation can include standard
20 carriers such as pharmaceutical grades of mannitol,
21 lactose, starch, magnesium stearate, sodium saccharine,
22 cellulose, magnesium carbonate, etc. Examples of
23 suitable pharmaceutical carriers are described in
24 "Remington's Pharmaceutical Sciences" by E.W. Martin.
25 Such compositions will contain a therapeutically
26 effective amount of the compound, preferably in purified
27 form, together with a suitable amount of carrier so as to
28 provide the form for proper administration to the
29 subject. The formulation should suit the mode of
30 administration.
31
32 In a preferred embodiment, the composition is formulated
33 in accordance with routine procedures as a pharmaceutical

1 composition adapted for intravenous administration to
2 human beings. Typically, compositions for intravenous
3 administration are solutions in sterile isotonic aqueous
4 buffer. Where necessary, the composition may also
5 include a solubilizing agent and a local anaesthetic such
6 as lidocaine to ease pain at the site of the injection.
7 Generally, the ingredients are supplied either separately
8 or mixed together in unit dosage form, for example, as a
9 dry lyophilized powder or water free concentrate in a
10 hermetically sealed container such as an ampoule or
11 sachette indicating the quantity of active agent. Where
12 the composition is to be administered by infusion, it can
13 be dispensed with an infusion bottle containing sterile
14 pharmaceutical grade water or saline. Where the
15 composition is administered by injection, an ampoule of
16 sterile water for injection or saline can be provided so
17 that the ingredients may be mixed prior to
18 administration.

19
20 The amount of the compound of the invention which will be
21 effective in the treatment of the conditions described
22 herein can be determined by standard clinical techniques
23 based on the present description. In addition, in vitro
24 assays may optionally be employed to help identify
25 optimal dosage ranges. The precise dose to be employed
26 in the formulation will also depend on the route of
27 administration, and the seriousness of the disease or
28 disorder, and should be decided according to the
29 judgement of the practitioner and each subject's
30 circumstances. However, suitable dosage ranges for
31 intravenous administration are generally about 20-500
32 micrograms of active compound per kilogram body weight.
33 Suitable dosage ranges for intranasal administration are

1 generally about 0.01 pg/kg body weight to 1 mg/kg body
2 weight. Effective doses may be extrapolated from
3 dose-response curves derived from in vitro or animal
4 model test systems.

5
6 The invention also provides a pharmaceutical pack or kit
7 comprising one or more containers filled with one or more
8 of the ingredients of the pharmaceutical compositions of
9 the invention. Optionally associated with such
10 container(s) can be a notice in the form prescribed by a
11 governmental agency regulating the manufacture, use or
12 sale of pharmaceuticals or biological products, which
13 notice reflects (a) approval by the agency of
14 manufacture, use or sale for human administration, (b)
15 directions for use, or both.

16
17 In a specific embodiment, it may be desirable to
18 administer the pharmaceutical compositions of the
19 invention locally to the area in need of treatment; this
20 may be achieved, for example, and not by way of
21 limitation, by local infusion during surgery or by
22 spraying the solution containing the lamellar bodies onto
23 the exposed tissue following surgery, by topical
24 application, by injection, by means of a catheter, or by
25 means of an implant, said implant being of a porous,
26 non-porous, or gelatinous material, including membranes,
27 such as sialastic membranes, or fibers or co-polymers
28 such as Elvax (see Ruan et al , 1992, Proc Natl Acad Sci
29 USA, 89:10872-10876). In one embodiment, administration
30 can be by direct injection by aerosol inhaler.

31
32 In yet another embodiment, the lamellar bodies can be
33 delivered in a controlled release system. In one

embodiment, a pump may be used (see Langer, supra; Sefton (1987) CRC Crit. Ref. Biomed. Eng. 14:201; Buchwald et al. (1980) Surgery 88:507; Saudek et al. (1989) N. Engl. J. Med. 321:574). In another embodiment, polymeric materials can be used (see Medical Applications of Controlled Release, Langer and Wise (eds.), CRC Pres., Boca Raton, Florida (1974); Controlled Drug Bioavailability, Drug Product Design and Performance, Smolen and Ball (eds.), Wiley, New York (1984); Ranger and Peppas, J. (1983) Macromol. Sci. Rev. Macromol. Chem. 23:61; see also Levy et al. (1985) Science 228:190; During et al. (1989) Ann. Neurol. 25:351; Howard et al. (1989) J. Neurosurg. 71:105). In yet another embodiment, a controlled release system can be placed in proximity of the therapeutic target, thus requiring only a fraction of the systemic dose (see, e.g., Goodson, in Medical Applications of Controlled Release (1984) supra, vol. 2, pp. 115-138). Other suitable controlled release systems are discussed in the review by Langer (1990) Science 249:1527-1533.

EXAMPLES

Example 1: Ex vivo investigation of effect of synthetic lamellar bodies on mucus, DNA, actin and alginate gels and ear wax.

Basic laboratory bench tests have been performed on the effect on the physical properties of linear macromolecules of the type involved in the pathophysiology of secretions and exudates when mixed with phospholipid microbodies (synthetic lamellar bodies).

1 **Materials**

2 The materials tested were chosen in the knowledge of the
3 probable molecular status of naturally-occurring polymers
4 in physiologic and in pathologic conditions. The range of
5 materials commercially available for selection was
6 however, restricted. Nevertheless, our accumulated
7 experience in this field directed that the main thrust of
8 the experiments on these gel-forming polymers would be
9 focused on demonstrating a molecular species interaction
10 between microbodies and polymers. In this regard it was a
11 basic premise of the experiments that the behaviour of
12 the gels was predictably similar, because of a shared
13 three-dimensional structure of this class of substances.
14 Thus the selection of mucus, DNA, actin and alginate
15 preparations were matched to the probable physical state
16 of the polymers in vivo.

17

18 Preparation of the gels, their range of concentration and
19 hydration was calculated to mimic as closely as possible
20 the putative range encompassing normal and pathological
21 conditions in humans.

22

23 **Characteristics of experimental mucus tested**

24 The mucus tested was derived from bovine, submaxillary
25 glands as supplied by Sigma (A70030). This is one of the
26 few commercially available products whose composition is
27 characterized. This particular agent has been tried and
28 tested in investigation of the physical characteristics
29 of the gel status of mucus in research on its viscosity
30 in inflammatory respiratory disorders, including CF.

31

32 In normal secretions, e.g. upper respiratory tract
33 surface fluid, mucus is present at low concentrations of

1 between 0.5% and 1% by weight. 99% of the secretions
2 consist of water containing electrolytes. Mucus has an
3 extended polypeptide backbone (apmucin) with numerous
4 oligosaccharide side-chains. Covered by abundant
5 polyanionic charges, mucus, on exocytotic release from
6 goblet cells, becomes extensively hydrated. Mucus then
7 forms a gel whose three-dimensional structure comprises a
8 tangled network of linear mucin polymers, devoid of
9 intermolecular cross-bridges. In certain situations of
10 hypersecretion and inflammation, the mucin concentration
11 can rise to 3%-5% by weight.

12
13 Mucus has low solubility. In bench-testing of the
14 physical properties of the bovine submaxillary mucus,
15 solutions up to a concentration of 5% were possible using
16 saline. For testing with lamellar bodies, concentrations
17 at 2.5% and 3.5% were employed to mimic those encountered
18 in pathological situations. Saline (0.9%) was used as the
19 diluent for all mucous samples tested.

20
21 Mucin monomers are polymerized through end-to-end
22 disulphide bonds to form linear polymers which, in
23 respiratory mucus, are at least 30μ long. These
24 dimensions should be viewed in context of the size of
25 lamellar bodies which range between 0.5μ - 2.0μ . Thus
26 lamellar bodies are of a dimension which can easily pass
27 through a tangled network of mucous "fibers" as observed
28 by light microscopy.

30 **Characteristics of experimental DNA tested**

31 The DNA chosen was polymeric in form and derived from
32 salmon testes (Sigma D1626). Like mucus, the DNA
33 preparation selected consists of linear polymers which

1 form a tangled "fibrous" gel. It is poorly soluble in
2 water and concentrations of over 5% by weight produce a
3 very stiff gel. In the tests carried out with lamellar
4 bodies, concentrations of 1% were regularly employed, and
5 the solvent used was always 0.9% saline. This
6 concentration of 1% was selected as probably being
7 representative of leucocyte (pus cells) and organismal-
8 derived DNA present in thick pathological secretions in
9 various disorders, ranging from CF through to chronic
10 otitis media.

11
12 A 1% solution of polymeric DNA in physiological saline is
13 a clear, syrupy liquid whose gel state possesses high
14 viscosity and adhesiveness.

15
16 **Characteristics of experimental combined mucus and DNA**
17 **gels**

18 Solutions of 2.5% mucus in 0.9% saline and 1% DNA in 0.9%
19 saline were made up separately. They were then carefully
20 mixed and stirred, avoiding the creation of bubbles. The
21 gels mixed well, without producing any changes in
22 turbidity. It is noteworthy that in published studies,
23 samples from patients of thick, viscous, infected
24 respiratory mucus when stained for DNA and mucus, showed
25 in wet preparations examined by confocal microscopy that
26 the different polymers were intimately mixed in the
27 three-dimensional structure of the gel. We were therefore
28 confident that the samples of combined mucus and DNA gel
29 prepared for testing with lamellar bodies were most
30 probably representative of viscous effusions in
31 pathological situations in a variety of in vivo
32 disorders, ranging from CF through to chronic otitis
33 media.

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Characteristics of synthetic lamellar bodies

The lamellar bodies tested were produced by the mixing of two organic solvents containing the phospholipids and cholesterol components. Based on analysis of lamellar bodies produced by human mesothelial cells, six constituents (five phospholipids and cholesterol) are used to make microbodies consisting of tightly-packed phospholipid bilayers with an ultrastructural geometry and periodicity (distance between bilayers) confirmed by electron microscopy to be identical to that of naturally-occurring lamellar bodies. The range of size of the synthetic lamellar bodies (0.2 - 3.5 μ m) was closely similar to that found in tissues and body cavities in man.

The lamellar bodies are made up in a physiological saline to a standard solution containing 10×10^9 microbodies per ml. The lamellar body density estimates are checked by turbidity comparison methods, while size distribution is obtained using flow cytometry.

Methods

Considering the widespread occurrence of mucus throughout the body, the literature on experimental work on its molecular biology is surprisingly scant. Current literature on the pathogenesis of cystic fibrosis admits ignorance of the basic pathogenetic mechanisms pertaining to mucus in different disorders. It is agreed by those in this field that investigation of visco-elastic properties of biological fluids and gels poses many technical and instrumental difficulties.

1 Applied viscometry has been developed exclusively for
2 industrial purposes, and all instruments are designed for
3 large fluid volumes. Pure biological polymers are
4 extremely expensive and measurement of multiple samples,
5 where minimal testing volumes per sample on available
6 instruments are 10-20ml, can be prohibitive.

7
8 Standard industrial viscometers employ mechanical
9 techniques, inducing shears, causing alignment of linear
10 polymers and thus disentangling the gel. Therefore,
11 measurement of biological gels in standard viscometers
12 (e.g. rotating disc and cone) can significantly alter the
13 viscosity of the sample during the test. On the other
14 hand, rheology of biological fluids has evolved using
15 instruments for investigation of blood which is a non-
16 Newtonian fluid. Likewise plasma viscosity is highly
17 dependent on globular, not linear, proteins like albumin
18 at 45g/l and globulin at 35g/l. Only one company
19 (recently disbanded) has designed instruments for
20 measurement of viscosity in biological fluids.

21
22 To obviate the difficulties in using instruments not
23 modified for testing viscosity in biological samples, a
24 series of pilot studies were carried out employing simple
25 devices to identify the most suitable method for
26 providing reliable measurements of change in viscosity in
27 gels mixed in saline with and without added lamellar
28 bodies.

29
30 A method was developed which measured distance travelled
31 in unit time by fixed volumes of test and control
32 samples, down a fixed incline under gravity (Galileo
33 technique), where the density and water content of the

1 samples were comparable, and the surface chosen was of
2 homogeneous composition, surface texture and charge. The
3 most appropriate slope tested was the surface of a
4 plastic Petri dish.

5
6 All laboratory ware used (i.e. containers, pipettes, etc)
7 were of plastics which did not contain plasticisers of
8 the type DEHP, since lamellar bodies leach out and are
9 altered by this plasticiser.

10
11 Gels were freshly made up to the appropriate
12 concentrations with adequate and careful mixing, ensuring
13 complete solubility and hydration of the polymers.

14
15 A measured volume of 0.9% saline containing lamellar
16 bodies was then added to test samples and an identical
17 volume of 0.9% saline only was added to the control
18 samples. Following careful, but complete mixing, samples
19 were incubated at 37°C for 1 hour.

20
21 After incubation and further careful mixing, droplets
22 (ranging from 30µl - 100µl) were accurately pipetted on a
23 start-line marked on the back of the Petri dish, which
24 also had a parallel "finish" line drawn at a distance of
25 5 cms. As the Petri dish was elevated to an angle of 90°,
26 an electronic stopwatch was triggered which was used to
27 record by observation the time taken for the droplet to
28 stream down to the 5 cm marker.

29 30 **Results**

31 The key elements of the findings are summarised in the
32 tables of Figures 1-3.

33

1 **Effect of varying concentrations of Lamellar bodies on**
2 **mucus gels**

3 The experiment most representative of the alterations
4 observed in the viscosity of mucus was the one
5 illustrated in Table 1 in which 3.5% mucus in saline was
6 sequentially diluted with increasing volumes of 0.9%
7 saline (controls) and 0.9% saline containing 10×10^9
8 lamellar bodies. The ratios of gel to diluent tested for
9 both test and control samples were 19:1, 9:1, 8:2, 7:3,
10 6:4.

11
12 No movement was observed in any of the samples in which
13 the diluent mixed with the mucus gel was physiological
14 saline only, in contrast to the test samples in which the
15 saline diluent contained lamellar bodies, where even at a
16 ratio of 19:1 there was significant movement in the
17 solution down the inclined plane. Thereafter, the speed
18 of travel increased steeply and at the ratio of nine
19 parts mucus to one part lamellar body solution, the fluid
20 travelled five centimetres in six seconds. At ratios of
21 seven parts to three, a maximum speed of travel was
22 reached at five centimetres per second. At these
23 concentrations the tests demonstrated highly significant
24 differences in the behaviour between the mucus gels mixed
25 with matched volumes of saline alone, compared with test
26 samples where the saline contained lamellar bodies. These
27 results tested within the stated range and concentrations
28 demonstrate that the presence of the phospholipid
29 microbodies confer a remarkable lubricity to the gel,
30 independent of the fluid content of the diluent.

31

32 **Effect of varying concentrations of Lamellar bodies on**
33 **DNA gels**

1 The experiment most representative of the alterations
2 observed in the viscosity of DNA was the one illustrated
3 in Table 2, one in which 1% DNA in saline was
4 sequentially diluted with increasing volumes of 0.9%
5 saline (controls) and 0.9% saline containing 10×10^9
6 lamellar bodies. The ratios of gel to diluent tested for
7 both test and control samples were 19:1, 9:1, 8:2, 7:3,
8 6:4, 5:5. Minimal movement was observed in both test and
9 control at dilutions from 19:1 down to 8:2. Thereafter,
10 test samples in which the diluent contained lamellar
11 bodies in ratios of 7:3, 6:4, 5:5 exhibited a steep
12 increase in speed of travel to 2.5 cms per second, as
13 compared to controls where the maximum speed was 5 cms in
14 4min 20sec.

15

16 **Effect of varying concentrations of Lamellar bodies on**
17 **combined DNA & mucus gels**

18 The experiment most representative of the alterations
19 observed in the viscosity of combined DNA and mucus gels
20 was the one illustrated in Table 3. The combined gel
21 consisted of 333 μ l of 2.5% mucus in 0.9% saline,
22 together with 333 μ l of 1% DNA in 0.9% saline. In the
23 control sample 333 μ l of 0.9% saline was added as
24 diluent, whereas in the test sample 333 μ l of saline
25 containing 10×10^9 lamellar bodies was added to the
26 combined gel. No movement was obtained in the control
27 sample, whereas the test sample containing lamellar
28 bodies travelled 5 cms in 2 sec at a speed of 2.5 cms per
29 sec. Therefore at a ratio of one third diluent containing
30 lamellar bodies added to two thirds combined mucus and
31 DNA gel, there was complete contrast between the fluidity
32 of the control and test sample.

33

1 **Alginate and actin gels**

2 Broadly similar results as those found in the testing of
3 the effect of lamellar bodies on mucus and DNA were
4 obtained in comparing their effect on alginate and actin
5 gels. The agents tested were muscle-derived, porcine
6 actin G (Sigma A0541) made up as a 0.5% solution in 0.9%
7 saline. Alginic acid, a polyuronic acid composed
8 primarily of anhydro-beta-D mannuronic acid residues with
9 1-4 linkage (Sigma A70030) was made up as a 2.5% solution
10 in 0.9% saline. Light microscopic observations showed
11 intimate mixing of lamellar bodies between the "fibers"
12 of the gels.

13

14 **Effect of lamellar bodies on mucus plugs blocking**
15 **tympanostomy tubes (vent tubes)**

16 In vitro laboratory experiments were carried out in which
17 vent tubes were filled with 5% mucus gel and allowed to
18 dry overnight. The tubes were inserted in the spigot of a
19 specially chosen 2ml syringe, whose conical profile
20 accommodated precisely the outer diameter of the vent
21 tube, to achieve complete occlusion. 0.5ml suspension of
22 lamellar bodies was pipetted into the barrel of the
23 syringe and its effect observed. Vent tubes were
24 unplugged at room temperature in a period that ranged
25 from 30-60 minutes. Saline controls had no effect after 6
26 hours.

27

28 **Effect of lamellar bodies on ear wax**

29 Human ear wax is a mixture of substances. The two main
30 constituents are desquamated squamous cells and cerumen.
31 The squamous epithelium which lines the external auditory
32 canal occupies an unusual position for skin. Over the
33 rest of the body the epidermis is renewed by constant

1 loss of surface cells and keratin by abrasion. Loss by
2 abrasion is not possible in the auditory canal. To
3 overcome this difficulty the surface epithelium
4 continually migrates centrifugally from the eardrum
5 outwards. Cerumen is a wax secreted by modified sweat
6 glands. These are situated in the sub-epidermal tissue
7 from where they discharge their secretion through ducts
8 onto the surface of the external auditory canal.

9

10 We have carried out tests in the laboratory on the effect
11 of lamellar bodies on samples of wax obtained from
12 patients, and have shown that the wax disintegrates over
13 a period ranging from 12 - 24 hours. Microscopic
14 observations on the process show penetration between the
15 plates of squames by lamellar bodies, lubricating and
16 separating the adhesive layers of dead cells which led to
17 disintegration of the wax.

18

19 **Conclusions**

20 The mixing of a saline solution containing lamellar
21 bodies with a mucus gel results in significant reduction
22 in the adhesiveness and viscosity of the mixture,
23 compared to a control mucus gel which has been mixed with
24 an equal volume of saline alone, when measured by rate of
25 movement down an inclined plane of identical composition,
26 surface texture and charge. Similar results were obtained
27 when lamellar bodies were added to DNA, actin and
28 alginate gels, and also to combined mucus and DNA gels.
29 Significant changes in speed of flow, and hence fluidity,
30 were encountered when the ratio of the volume of standard
31 solution containing lamellar bodies added to the gel was
32 around 3 to 7.

33

CLAIMS:

1. Use of a composition comprising a therapeutically effective amount of lamellar bodies and a pharmaceutically acceptable carrier to modify linear biological macromolecules of the type mucins, DNA, actin and bacterial-derived alginate, for treating a disease state characterized by mucous secretions.
2. The use as claimed in claim 1, wherein the disease state characterized by mucous secretions is selected from the group consisting of acute and chronic otitis media, cystic fibrosis, bronchitis, bronchiectasis, sinusitis, nasal congestion, asthma, chronic obstructive pulmonary disease, disorders of the genito-urinary tract, hepato-biliary disorders, blockage and/or loculation of fistula lumen, pancreatic and reproductive tract disorders, thermal and radiation burns, chronic ulcers, de-gloving injuries, pathological conditions wherein the surface of the eye becomes dry and/or covered by thickened viscous secretions or exudates, and mucositis.
3. The use as claimed in claim 1, wherein the disease state characterized by mucous secretions is selected from the group consisting of otitis media, cystic fibrosis, bronchitis, sinusitis, nasal congestion, asthma, bronchiectasis, chronic obstructive pulmonary disease, hepato-biliary disorders, pancreatic and reproductive tract disorders and mucositis.
4. The use as claimed in claim 1, for modifying the viscosity and adhesiveness of the linear biological macromolecules to increase the fluidity of a subject's airway surface fluid and restore mucociliary clearance of the linear biological macromolecules throughout the respiratory tract.

5. The use of any one of claims 1 to 4, wherein the lamellar bodies comprise phosphatidylcholine, sphingomyelin, phosphatidyl ethanolamine, phosphatidyl serine, phosphatidyl inositol and cholesterol.
6. The use of any one of claims 1 to 5, wherein said lamellar bodies comprise:
about 44-70% phosphatidylcholine,
about 15-23% sphingomyelin,
about 6-10% phosphatidyl ethanolamine,
about 2-6% phosphatidyl serine,
about 2-4% phosphatidyl inositol, and
about 4-12% cholesterol, by weight.
7. The use of any one of claims 1 to 6, wherein said composition further comprises above 0 to about 3% by weight of lysophosphatidyl choline.
8. The use of any one of claims 1 to 7, wherein said lamellar bodies comprise:
about 54% phosphatidylcholine,
about 19% sphingomyelin,
about 8% phosphatidyl ethanolamine,
about 4% phosphatidyl serine,
about 3% phosphatidyl inositol, and
about 10% cholesterol, by weight.
9. The use of claim 8, wherein said composition further comprises about 2% by weight of lysophosphatidyl choline.
10. The use of any one of claims 1 to 9 further comprising therapeutic moieties in combination with the lamellar bodies.

11. The use of any one of claims 1 to 10, wherein the lamellar bodies in the composition are suspended lamellar bodies and the composition is in the form of an aerosol spray.
12. The use of claim 11, wherein the suspended lamellar bodies may be subjected to ultrasonification during administration of inhaled aerosol.
13. The use as claimed in any one of claims 1 to 10, wherein the lamellar bodies in the composition are delivered in a controlled release system.
14. The use as claimed in any one of claims 1 to 10 comprising a dosage form of lamellar bodies in a physiological saline containing 10×10^9 microbodies per ml.

<u>CONTROL</u>			<u>TEST</u>		
3.5% Mucus in 0.9% saline : saline diluent 0.9% saline			3.5% Mucus in 0.9% saline : Synthetic lamellar bodies in 0.9% saline		
Volume & Concentration	Dilution	Time to Travel	5cms	Dilution	Volume & Concentration
950 µl mucus + 50 µl NaCl	19:1	No movement @ 5 min	3m 50sec	19:1	950 µl mucus + 50 µl LMS
900 µl mucus + 100 µl NaCl	9:1	No movement @ 5 min	6 sec	9:1	900 µl mucus + 100 µl LMS
800 µl mucus + 200 µl NaCl	8:2	No movement @ 5 min	2 sec	8:2	800 µl mucus + 200 µl LMS
700 µl mucus + 300 µl NaCl	7:3	No movement @ 5 min	1 sec	7:3	700 µl mucus + 300 µl LMS
600 µl mucus + 400 µl NaCl	6:4	No movement @ 5 min	1 sec	6:4	600 µl mucus + 400 µl LMS

Table 1: Effect of varying concentrations of synthetic lamellar bodies on mucus fluidity compared with use of saline diluent as control. Each sample tested was exactly 30µl. The angle of incline was 90°

Fig. 1

<u>CONTROL</u>			<u>TEST</u>		
1% DNA in 0.9% saline : diluent 0.9% saline			1% DNA IN 0.9% saline : Synthetic lamellar bodies in 0.9% saline		
Volume & Concentration	Dilution	Time to Travel	5 cms	Dilution	Volume & Concentration
950 µl DNA + 50 µl NaCl	19:1	10mm @ 5 min	11mm @ 5 min	19:1	950 µl DNA + 50 µl LMS
900 µl DNA + 100 µl NaCl	9:1	10mm @ 5 min	11mm @ 5 min	9:1	900 µl DNA + 100 µl LMS
800 µl DNA + 200 µl NaCl	8:2	25mm @ 5 min	31 mm @ 5 min	8:2	800 µl DNA + 200 µl LMS
700 µl DNA + 300 µl NaCl	7:3	45mm @ 5 min	22 sec	7:3	700 µl DNA + 200 µl LMS
600 µl DNA + 400 µl NaCl	6:4	4 min 20 sec	2 sec	6:4	600 µl DNA + 200 µl LMS
500 µl DNA + 500 µl NaCl	5:5	2 min 32 sec	2 sec	5:5	500 µl DNA + 500 µl LMS

Table 2: Effect at 37°C of varying concentrations of synthetic lamellar bodies on DNA fluidity compared with use of saline diluent as control.
Each sample tested was 100 µl. The angle of incline was 90 °.

Fig. 2

<u>CONTROL</u>	<u>TIME TO TRAVEL 5 CMS</u>		<u>TEST</u>
333 µl 2.5% mucus in 0.9% saline	2 sec	No movement	333 µl 2.5% mucus in 0.9% saline
333 µl 1% DNA in 0.9% saline		@ 5 min	333 µl 1% DNA in 0.9% saline
333 µl 0.9% saline as diluent			333 µl LMS in 0.9% saline

Table 3: Effect at 37°C of synthetic lamellar bodies on fluidity of a combined mucus – DNA gel at a ratio of one third volume synthetic lamellar bodies to two thirds DNA & mucus gel compared with control using one third volume of 0.9% saline. Each sample tested was 40 µl. The angle of incline was 90°

Fig. 3