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(54) **LATERALLY INSERTABLE ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH TRANSLATING PIVOT POINT**

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Related U.S. Application Data

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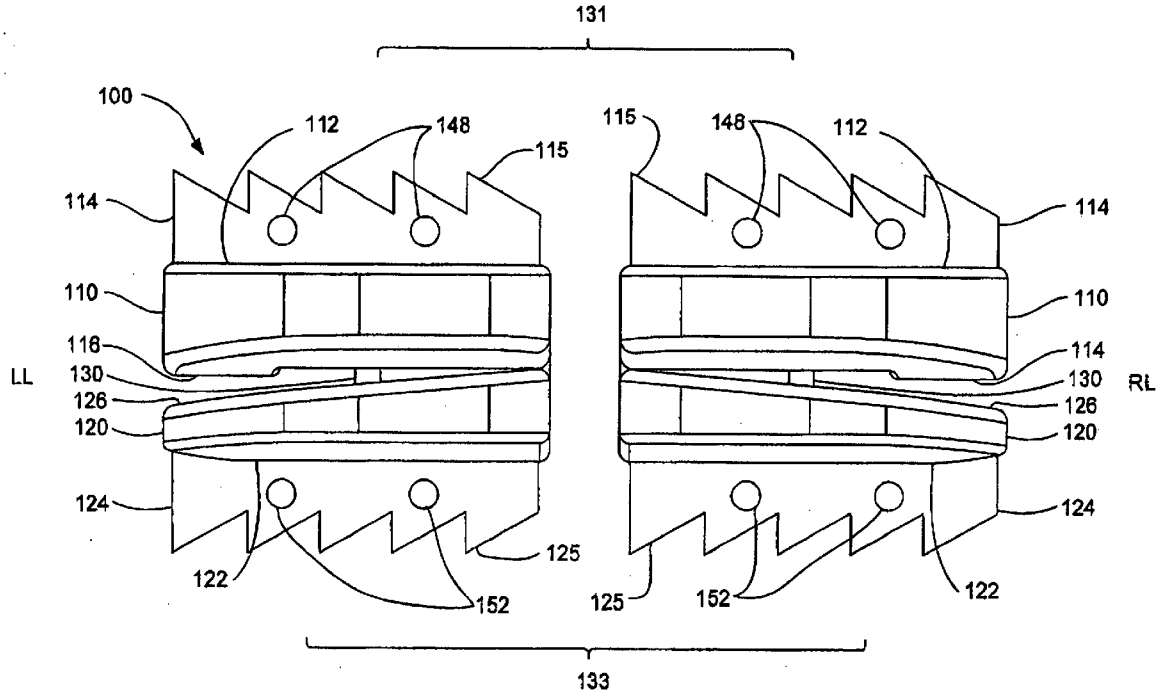
Publication Classification

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(52) **U.S. Cl.** **623/17.15**

(57) **ABSTRACT**

An implant that can be placed between two vertebrae using a lateral insertion method is described. The implant is characterized by having a first end plate and a second end plate with a hemi-cylindrical spacer extending from the second end plate. The hemi-cylindrical spacer fits within a socket on the first end plate and allows for pivotal or rotational motion and also for twisting motion.



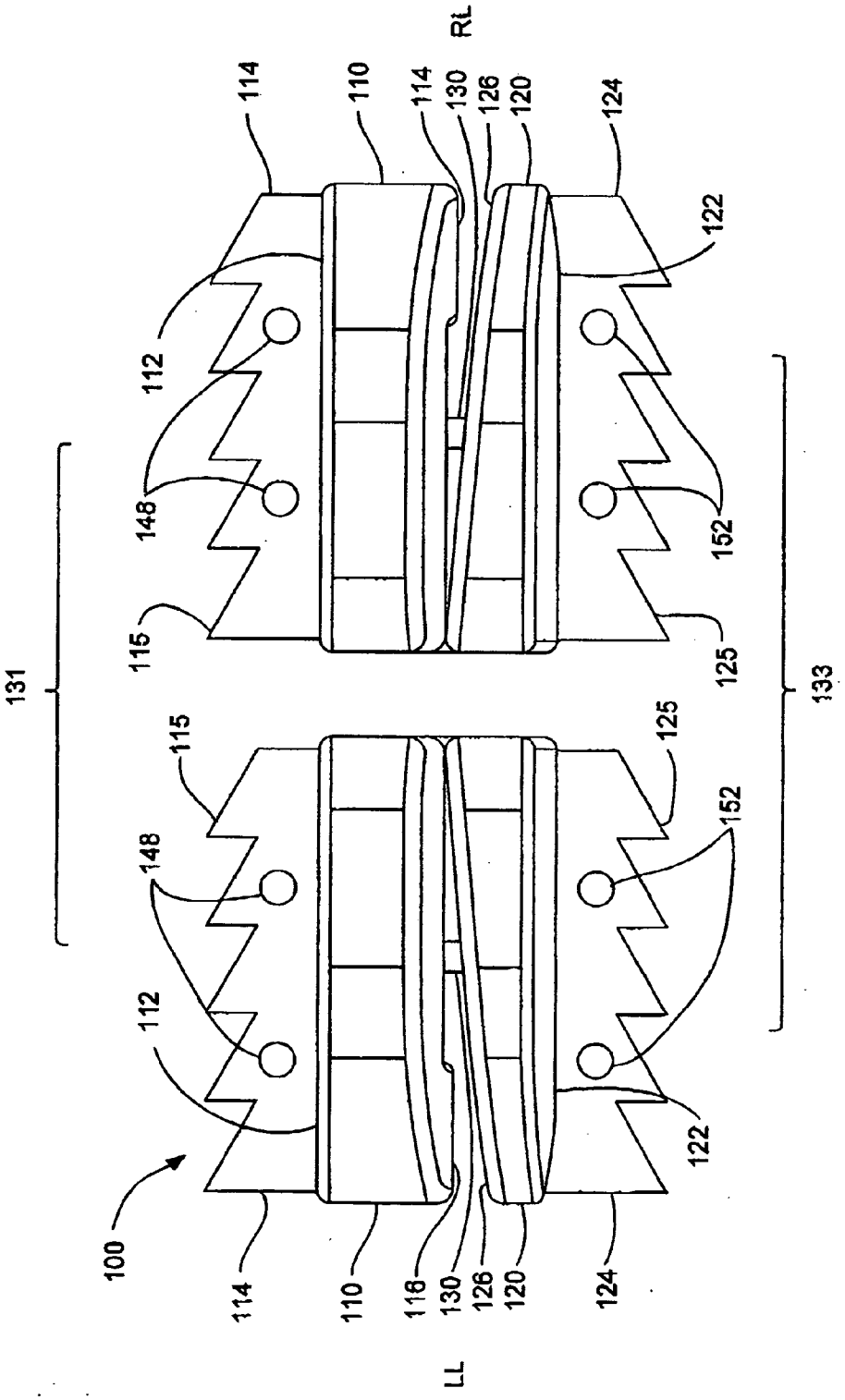

RL
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FIG. - 1A

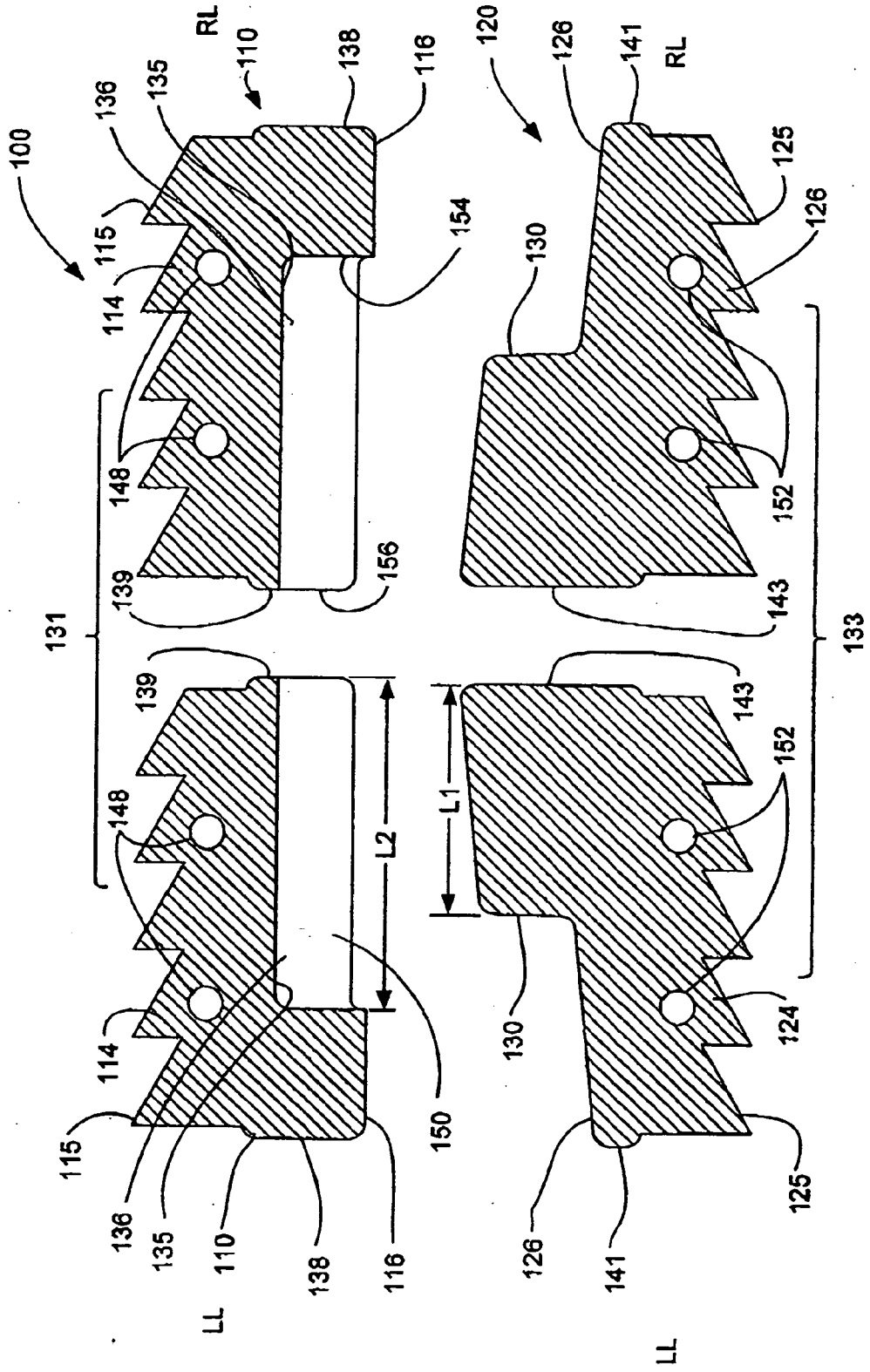

100
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120
126
141
RL
136
135
138
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154
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148
152
139
156
143
131
133
L1
L2
150
124
LL
LL

FIG. - 1B

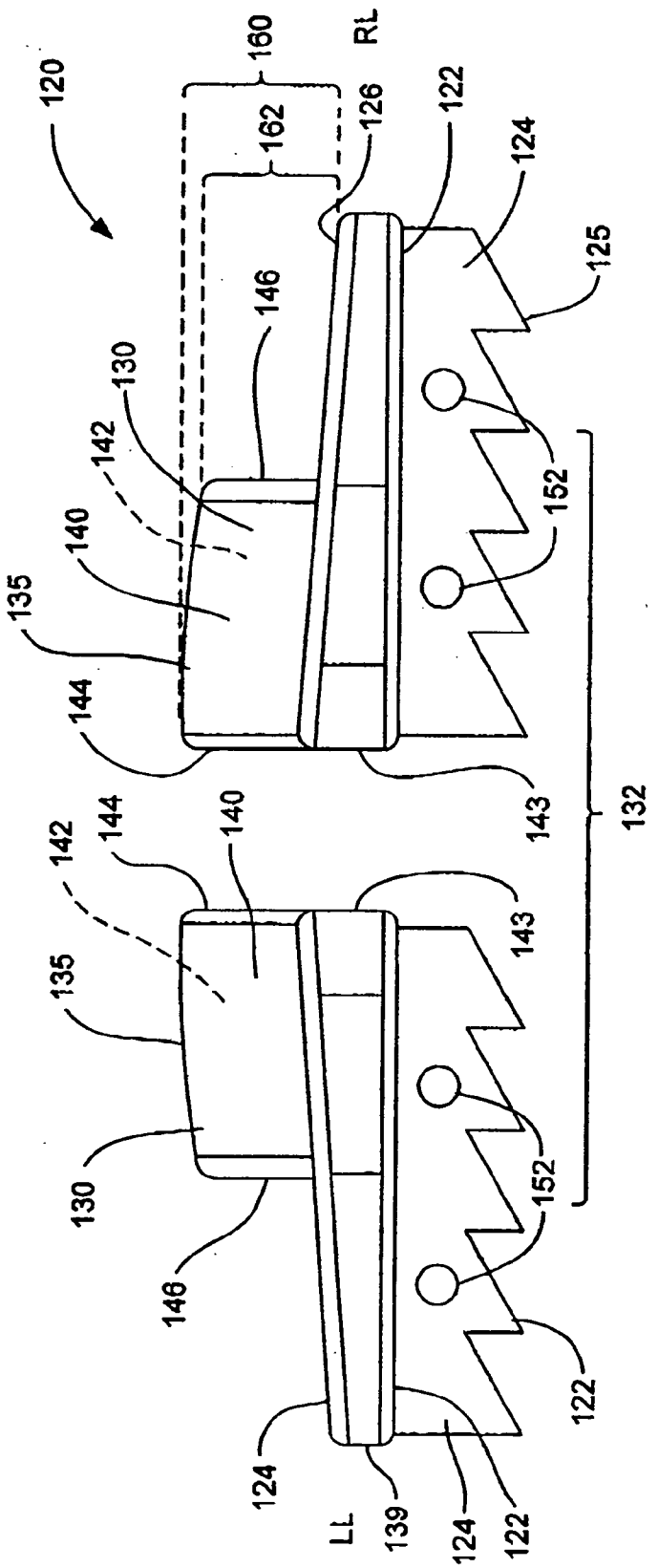

120
160
RL
162
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132
LL
139

FIG. - 1C

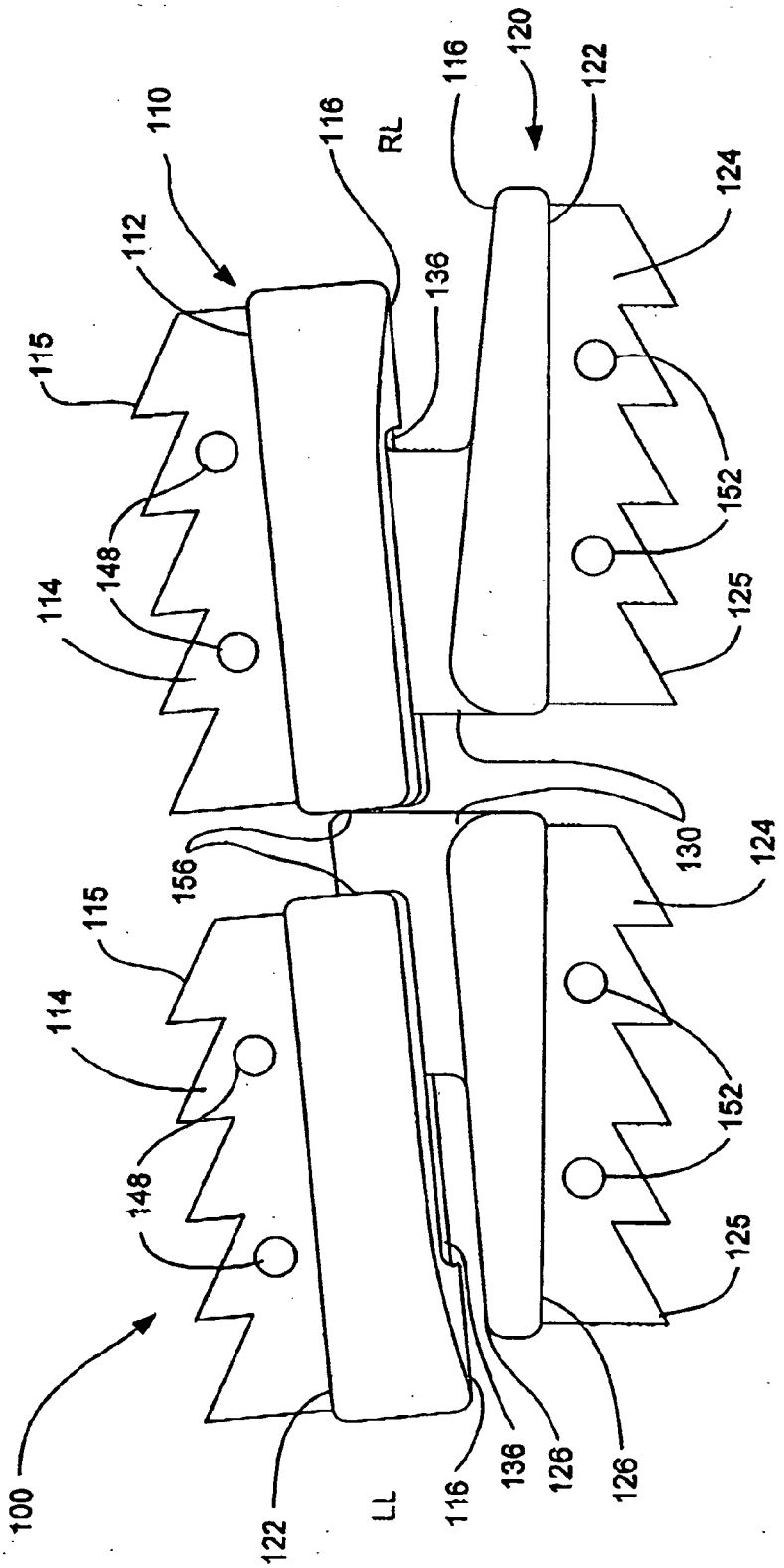

100
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FIG. - 1D

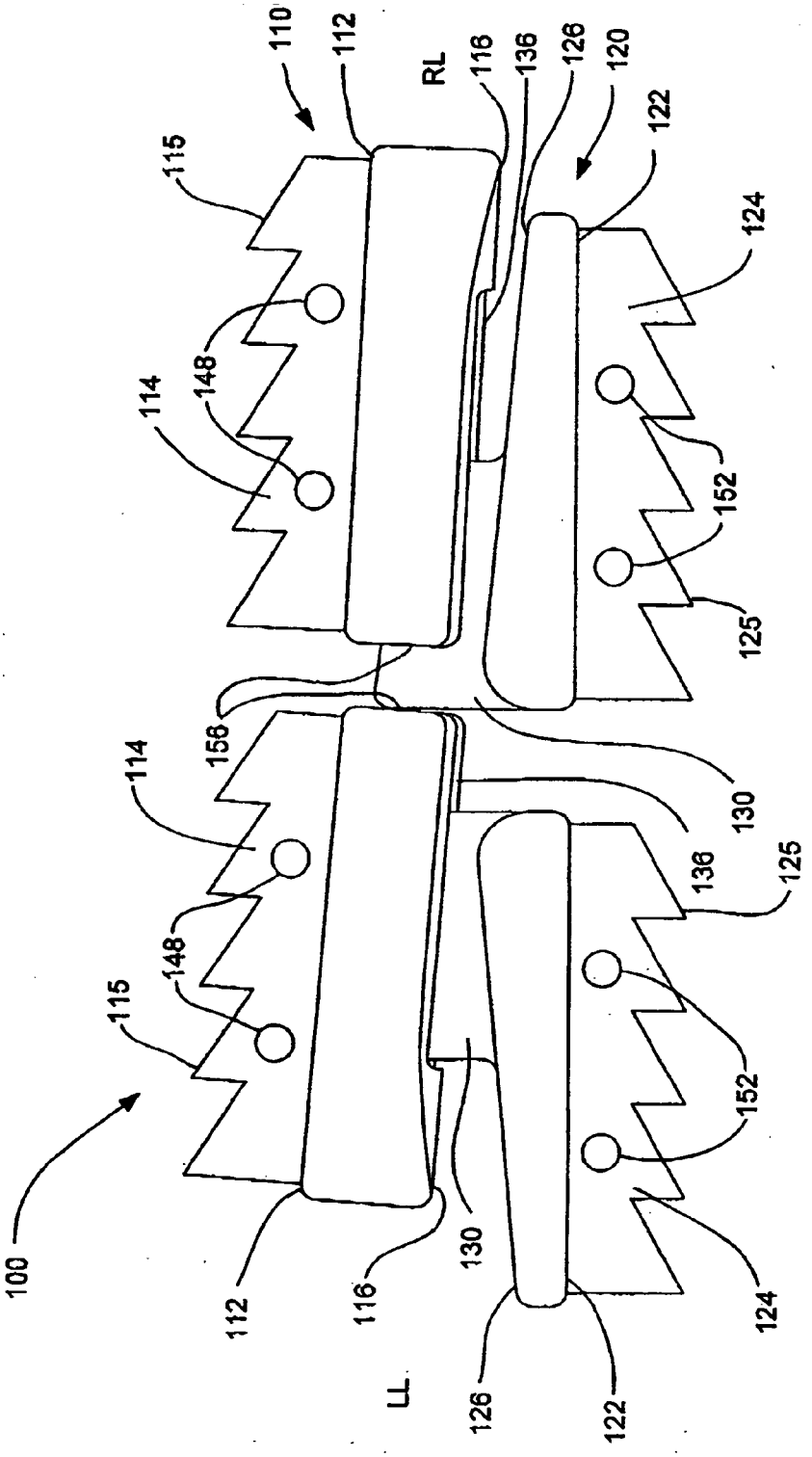

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LL
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FIG. - 1E

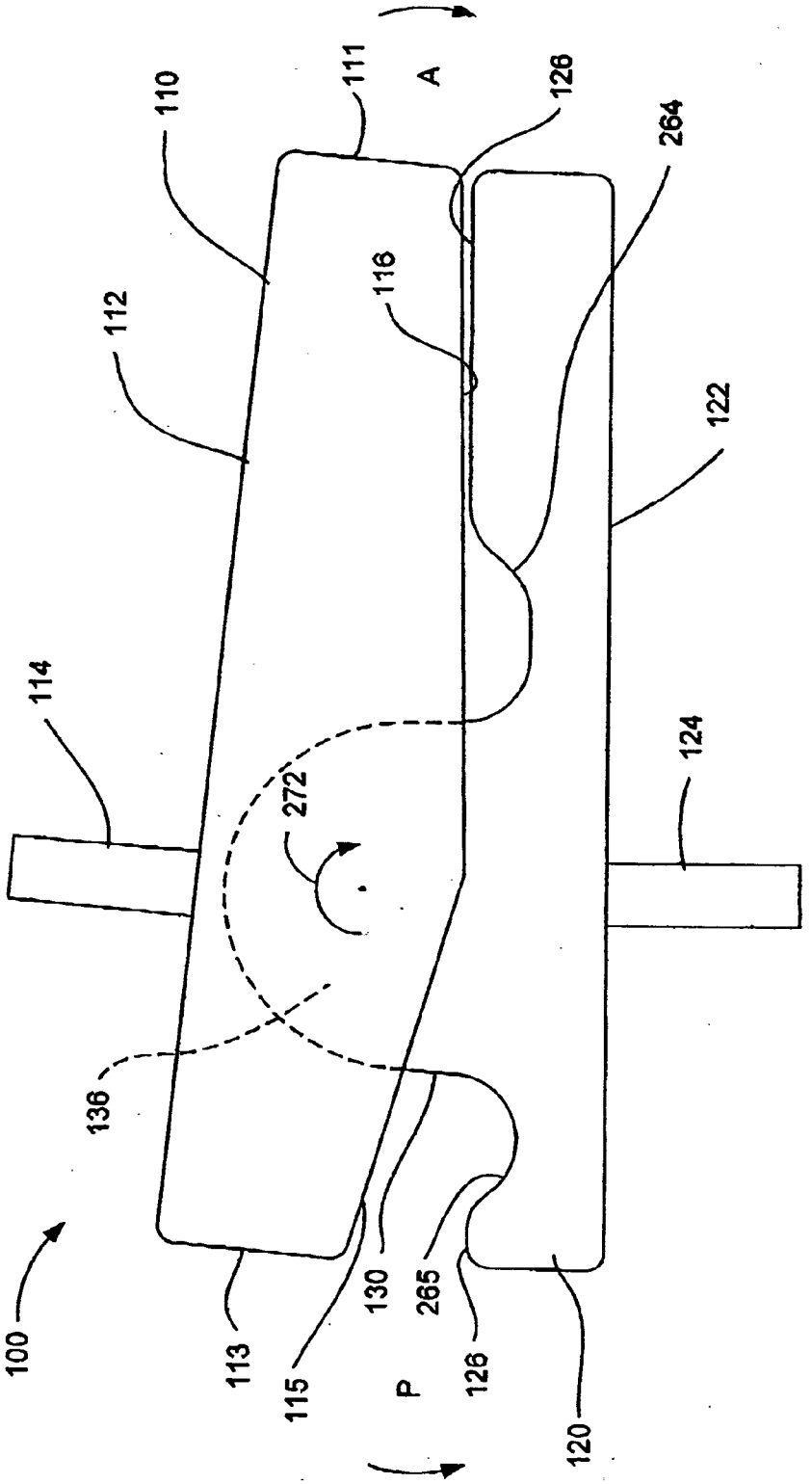

110
111
A
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264
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272
136
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265
126
P
120

FIG. - 2A

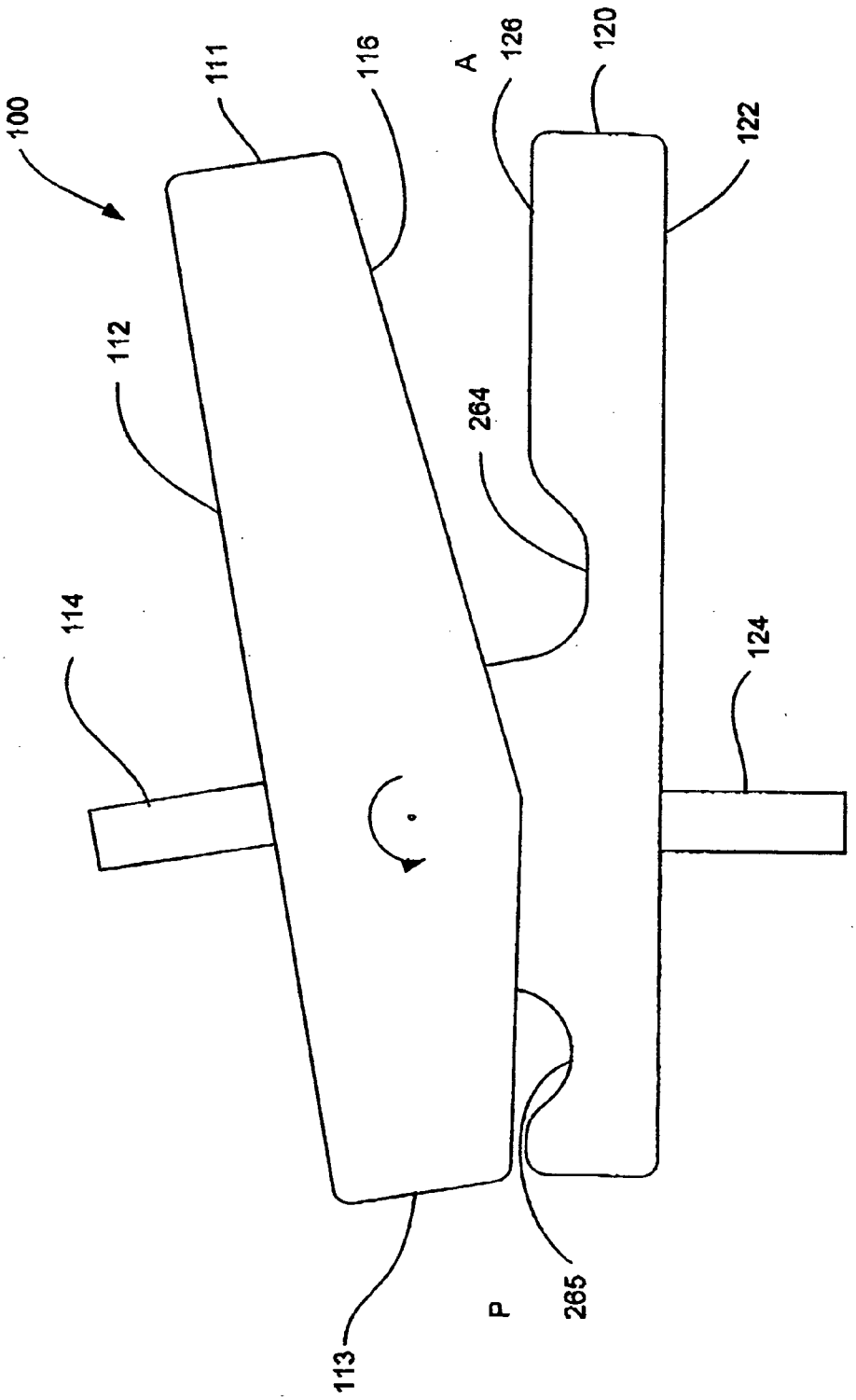


FIG. - 2B

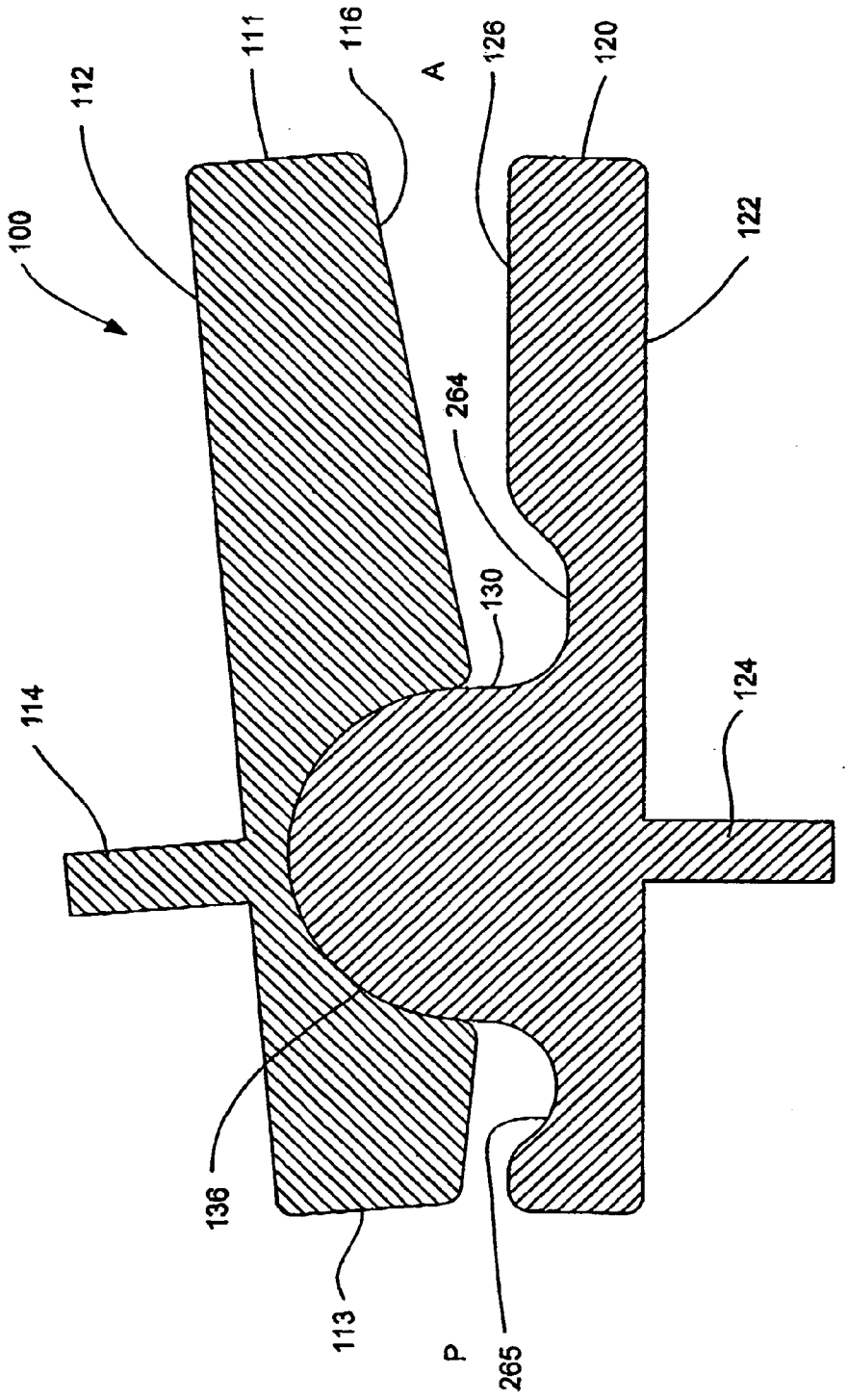


FIG. - 2C

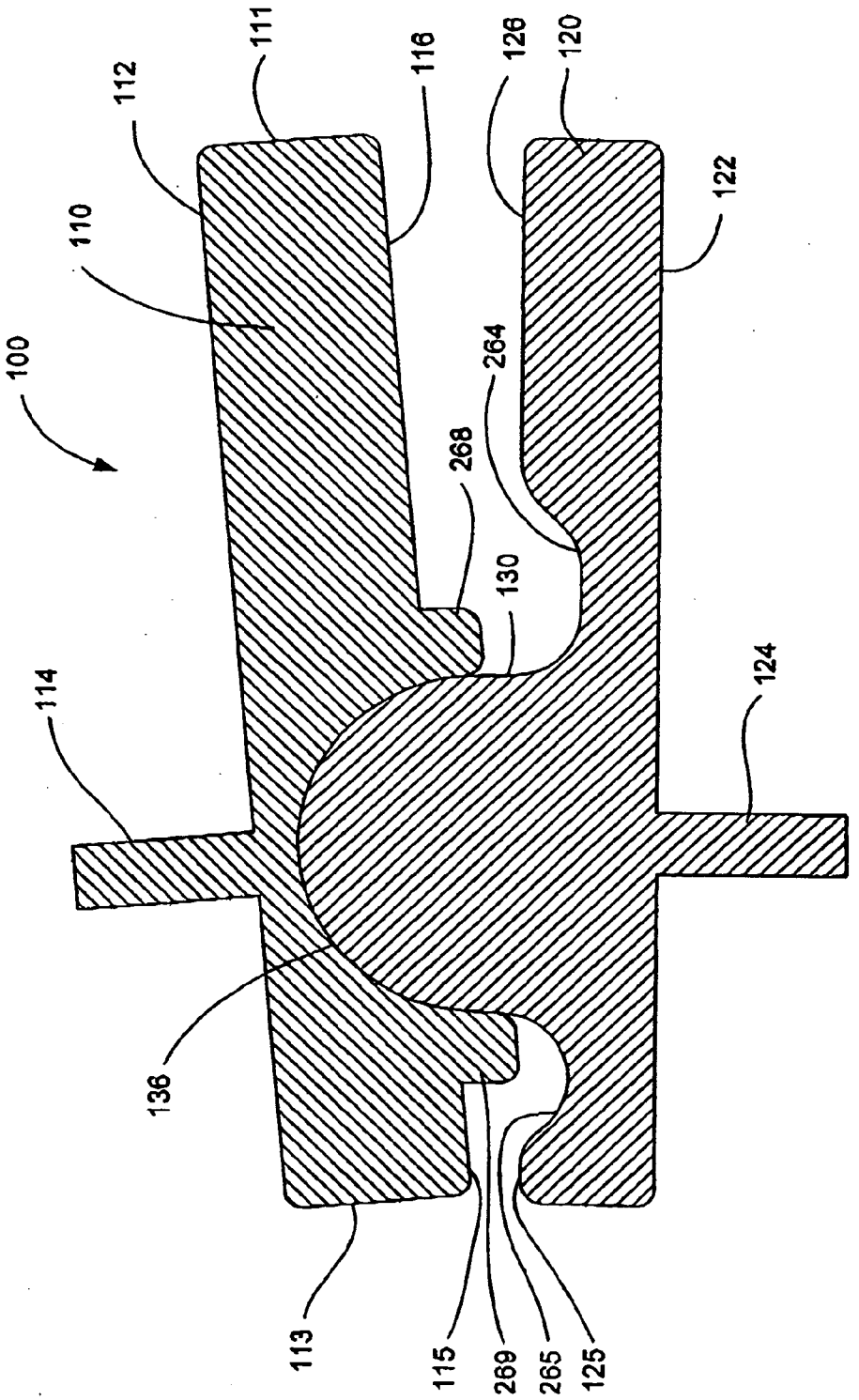

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FIG. - 2D

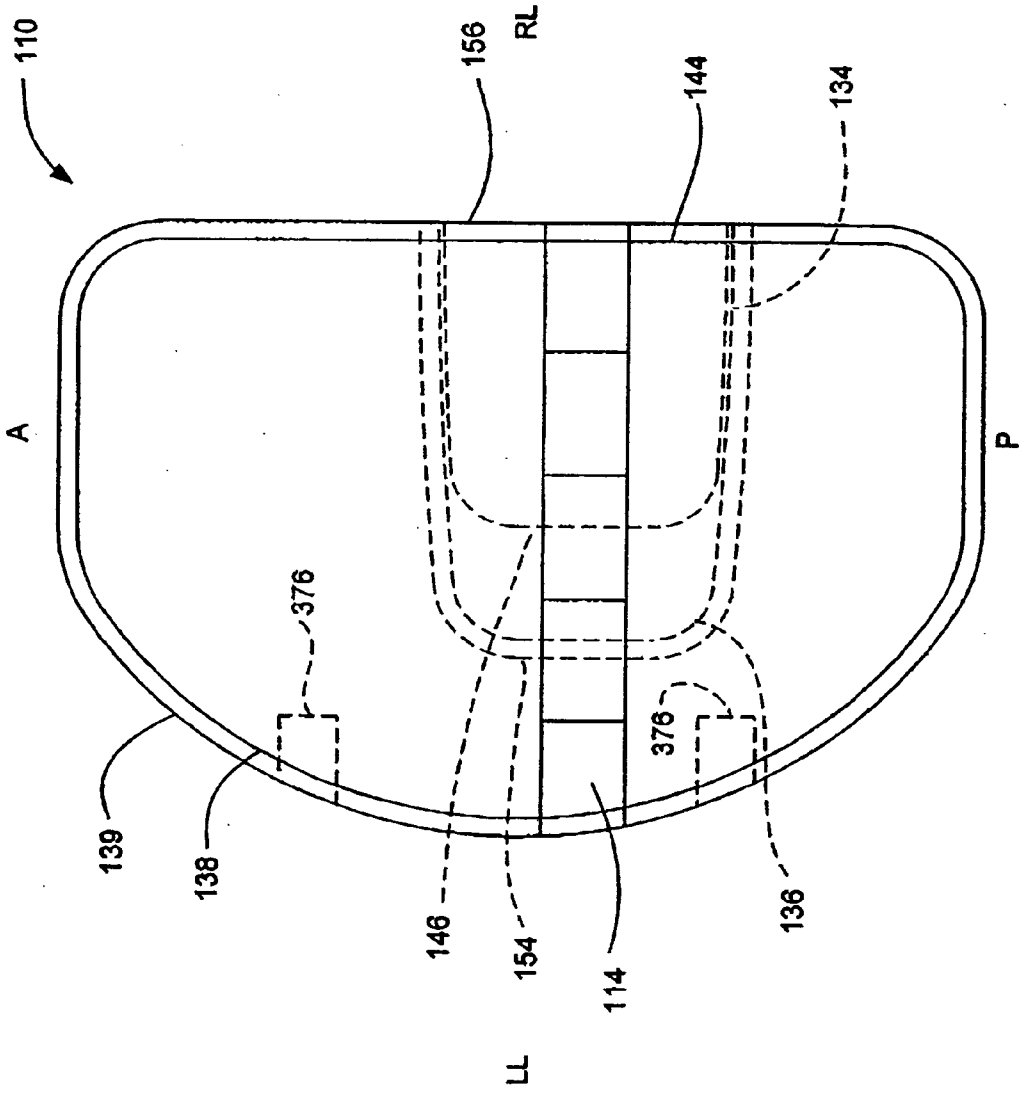


FIG. - 3A

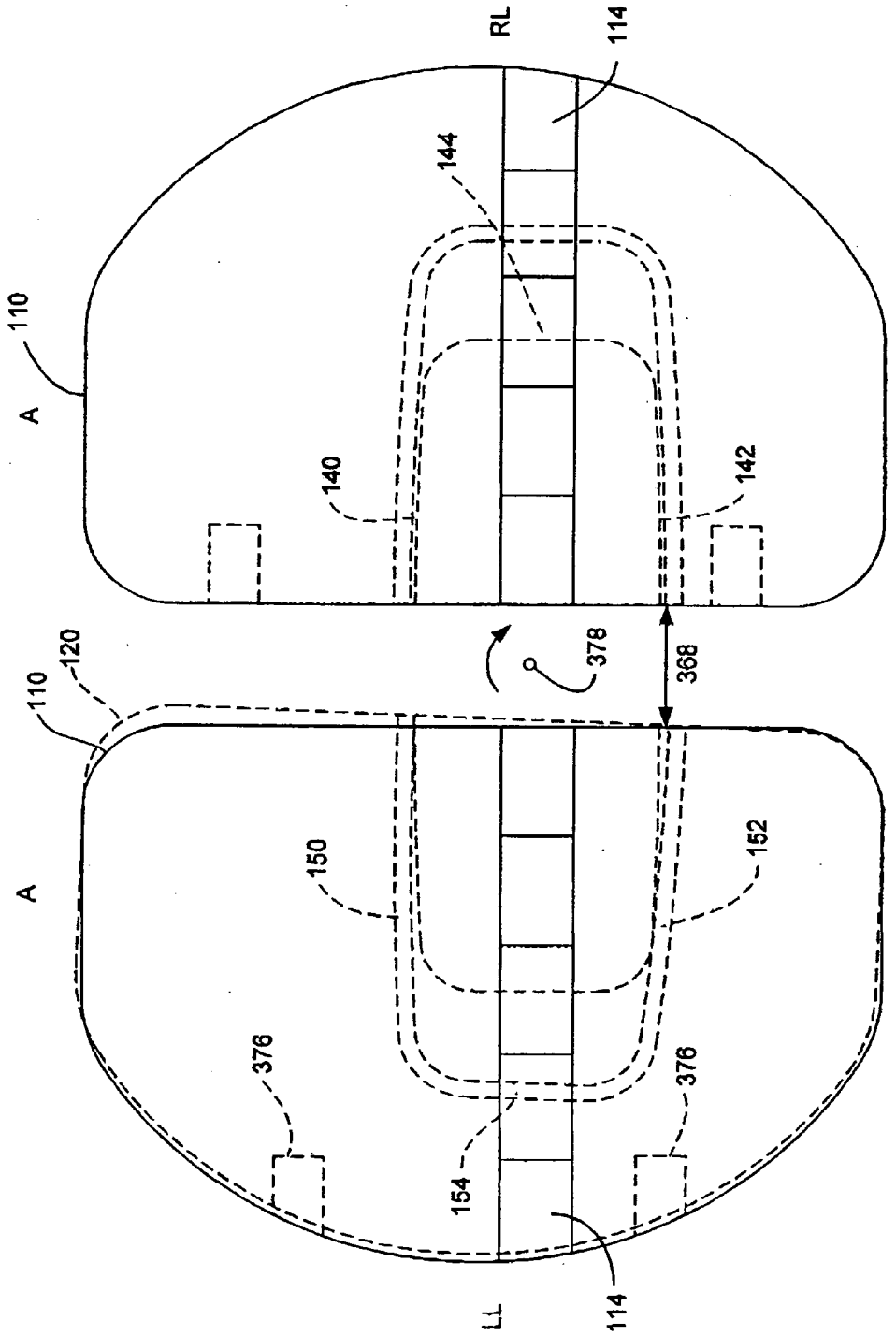

RL
114
144
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A
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142
P
378
368
120
110
A
150
152
376
376
154
LL
114
P

FIG. - 3B

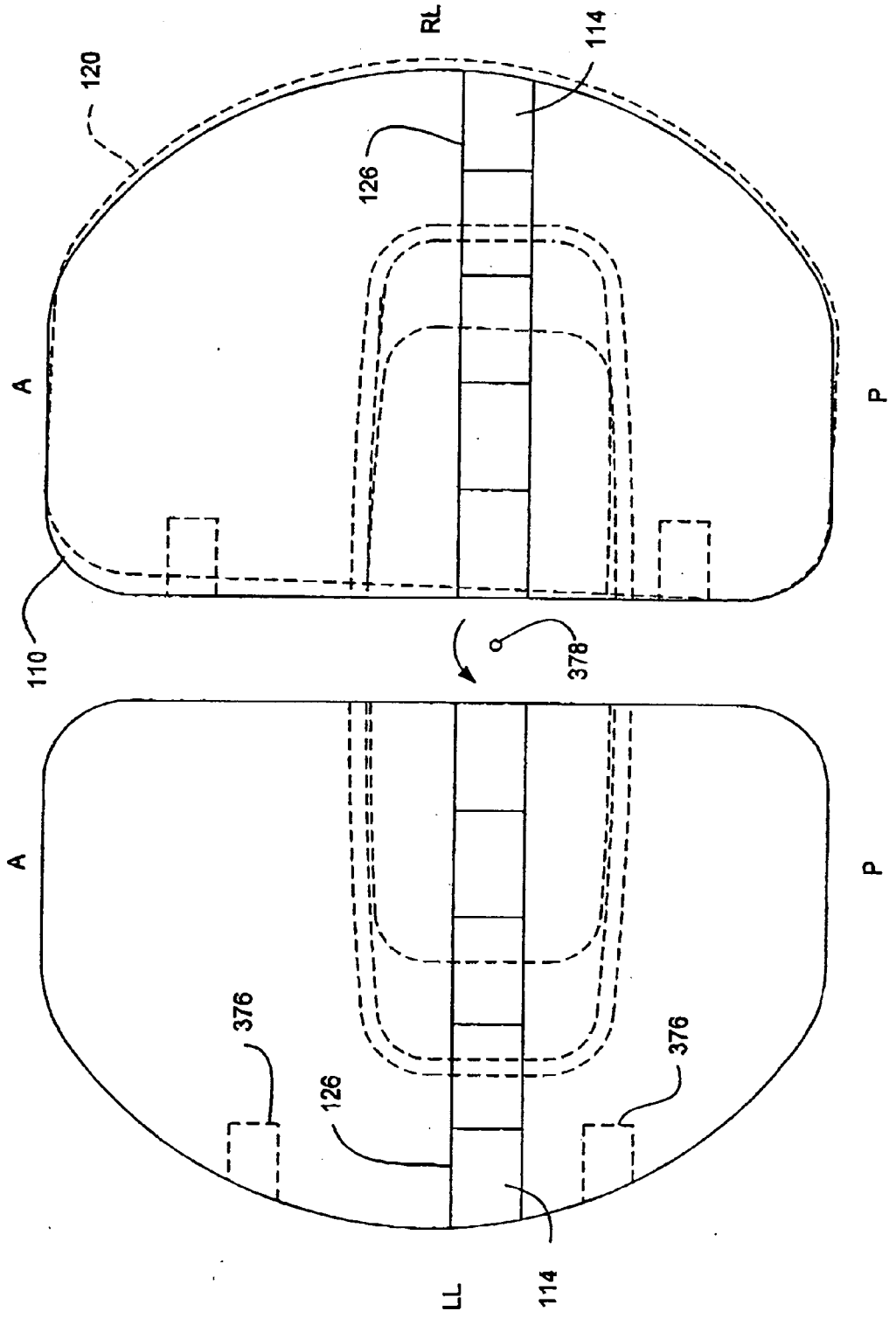


FIG. - 3C

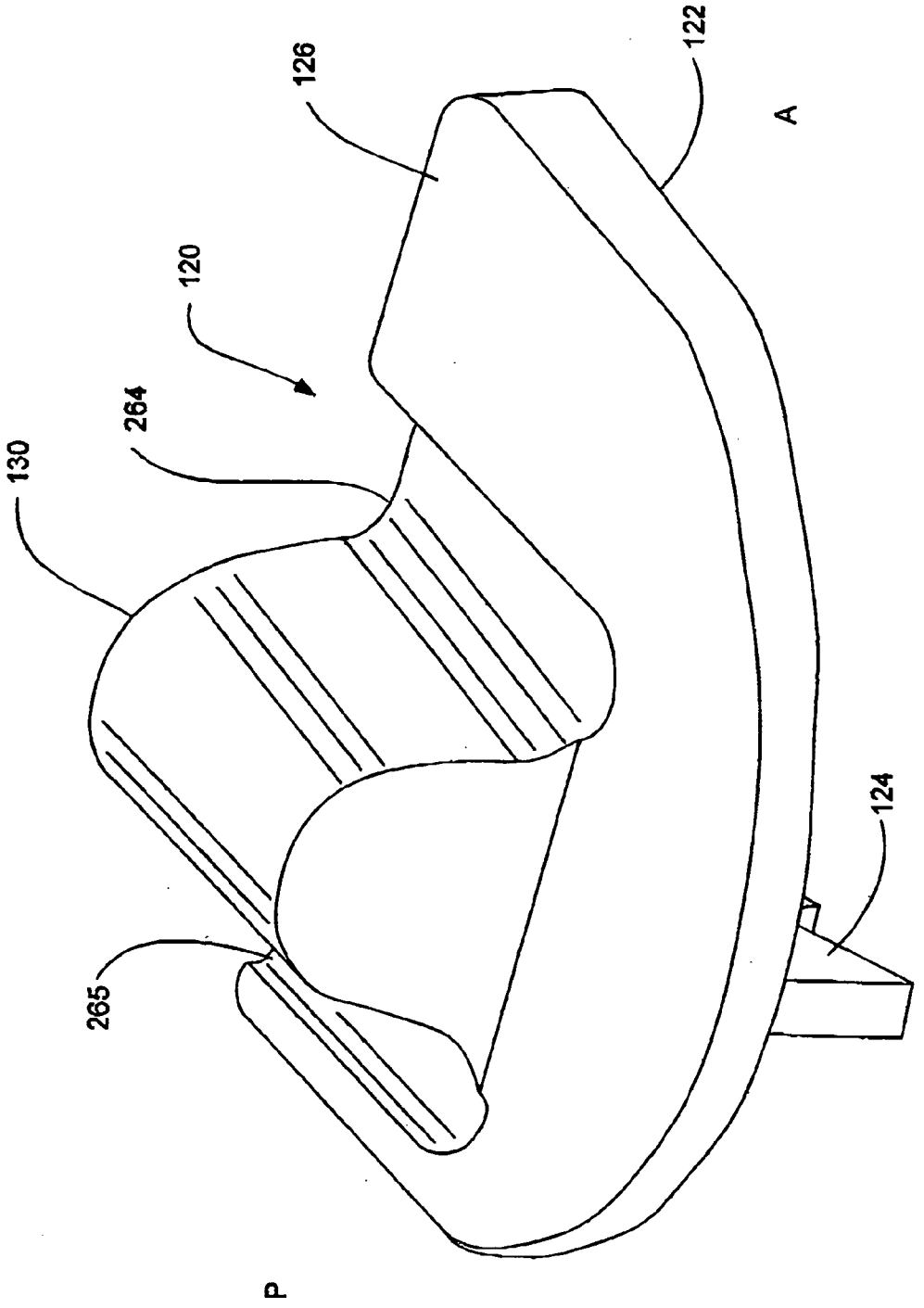


FIG. - 4A

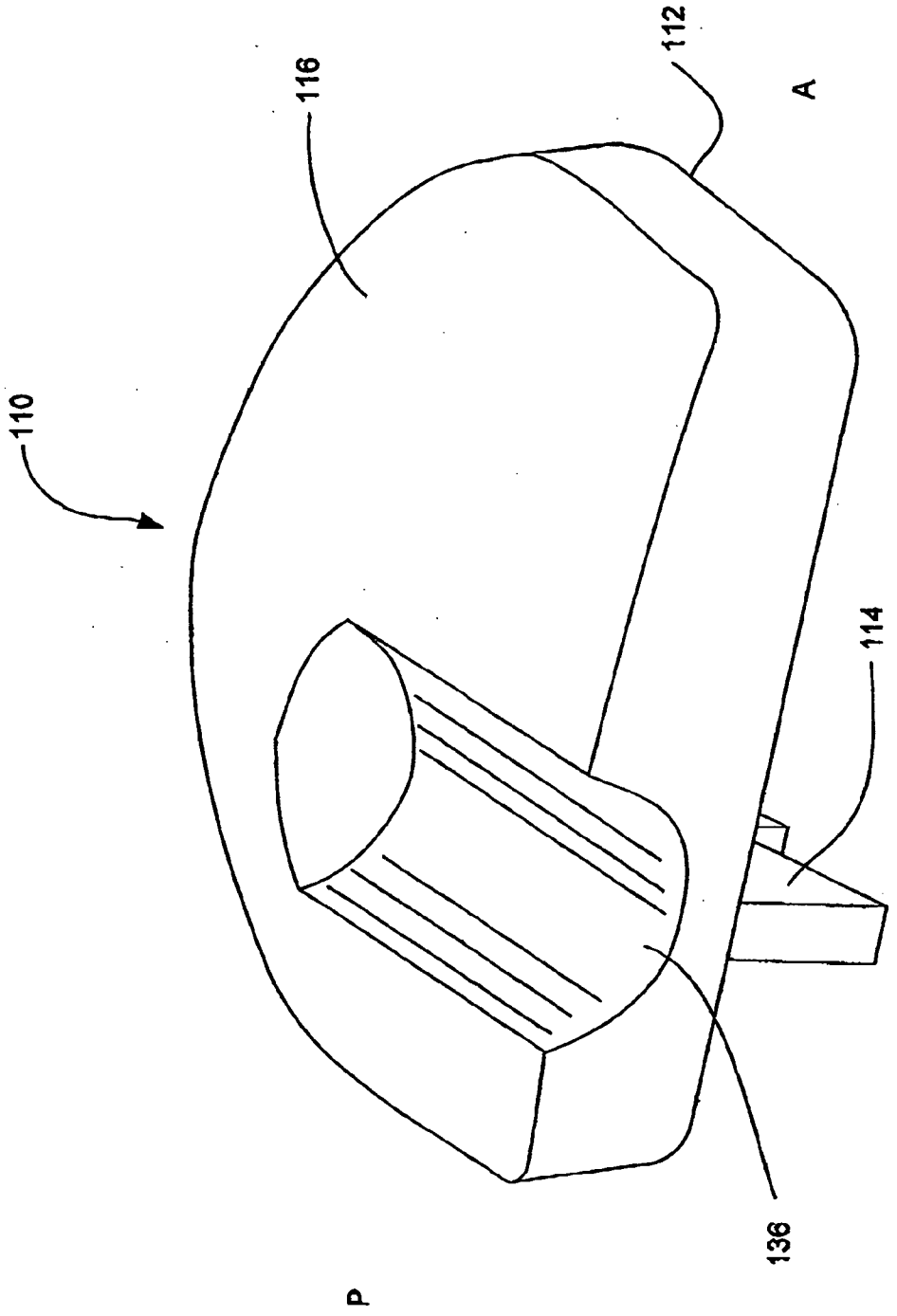


FIG. - 4B

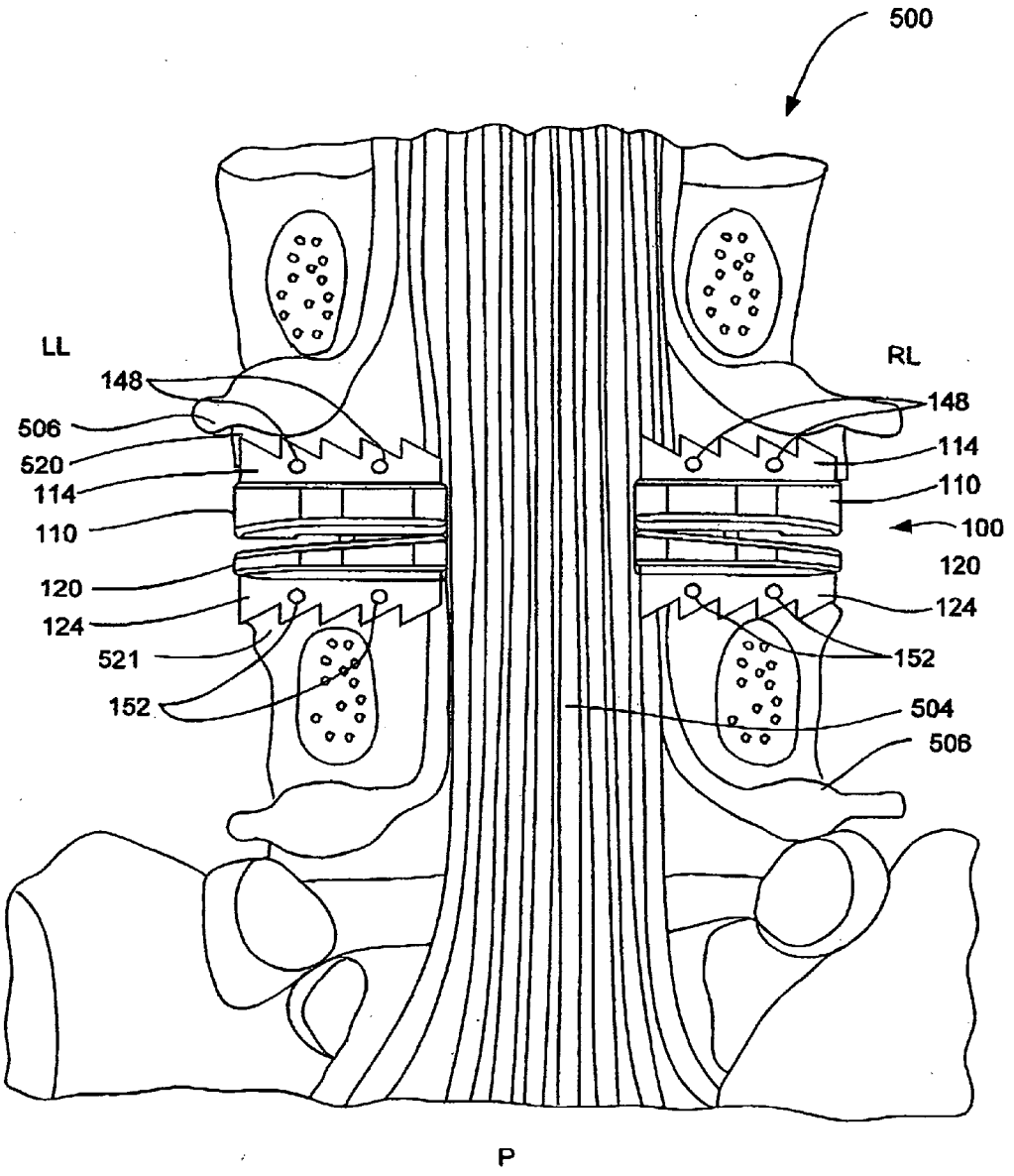

500
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FIG. - 5A

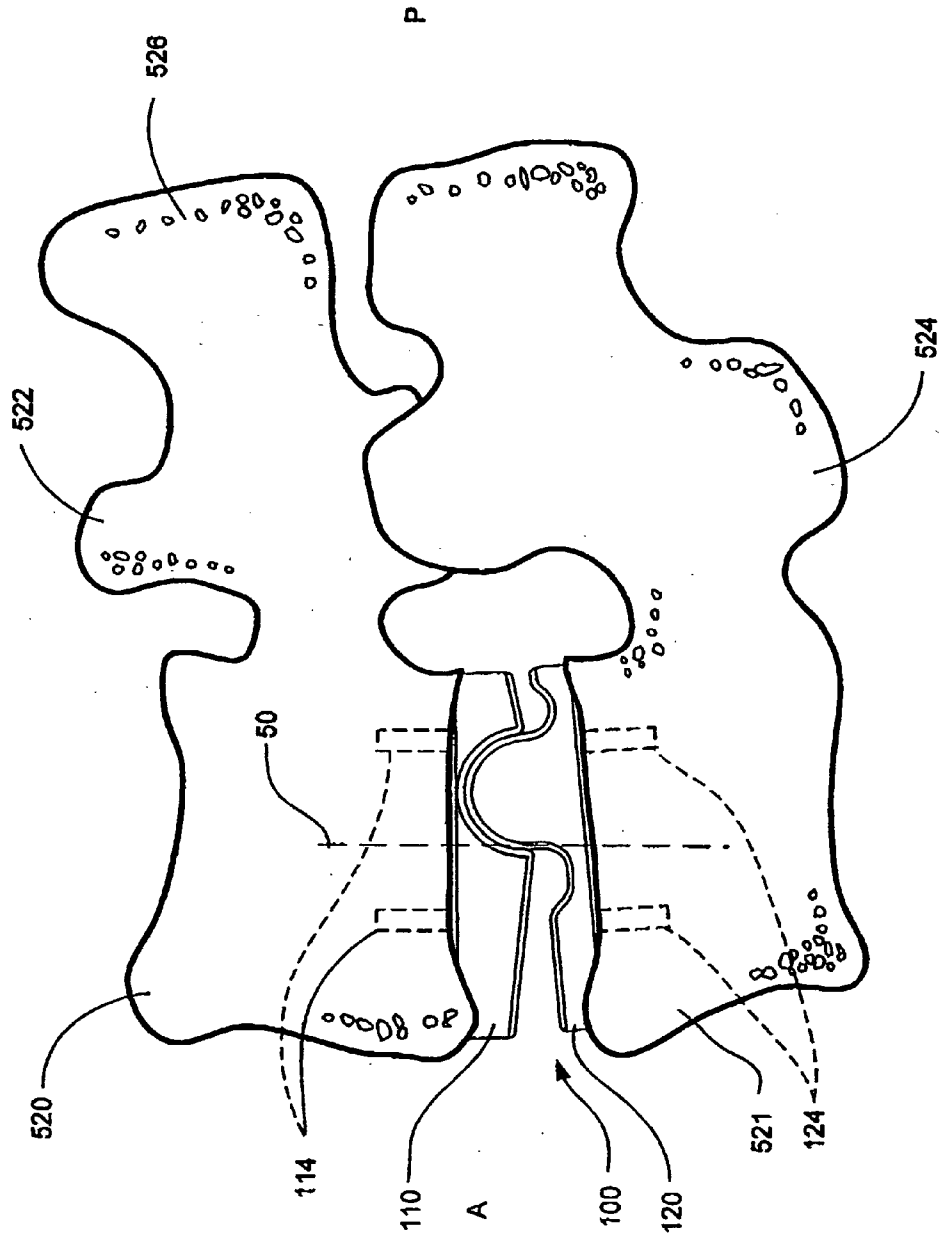


FIG. - 5B

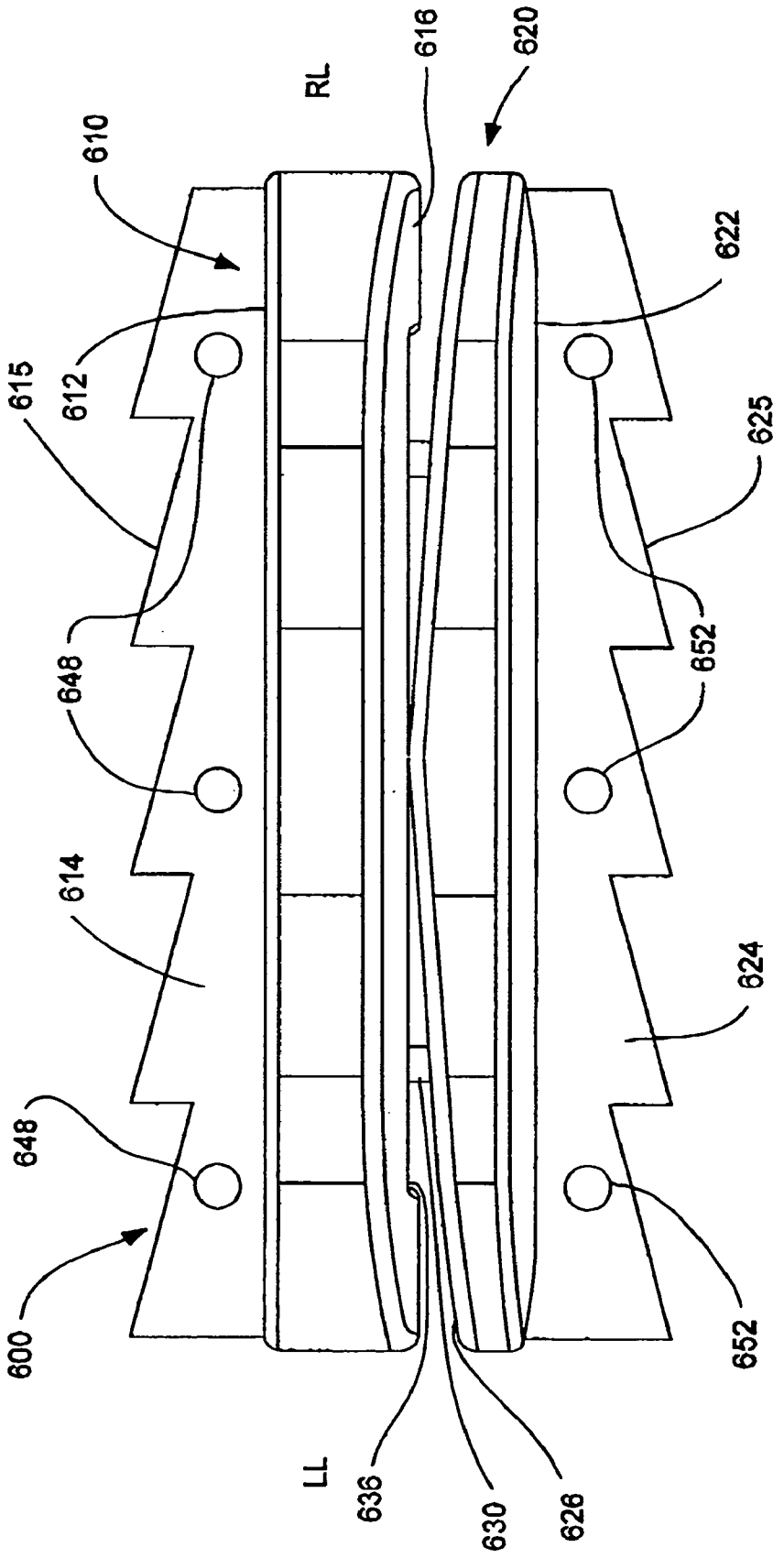

RL
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600
652
LL
636
630
626

FIG. - 6A

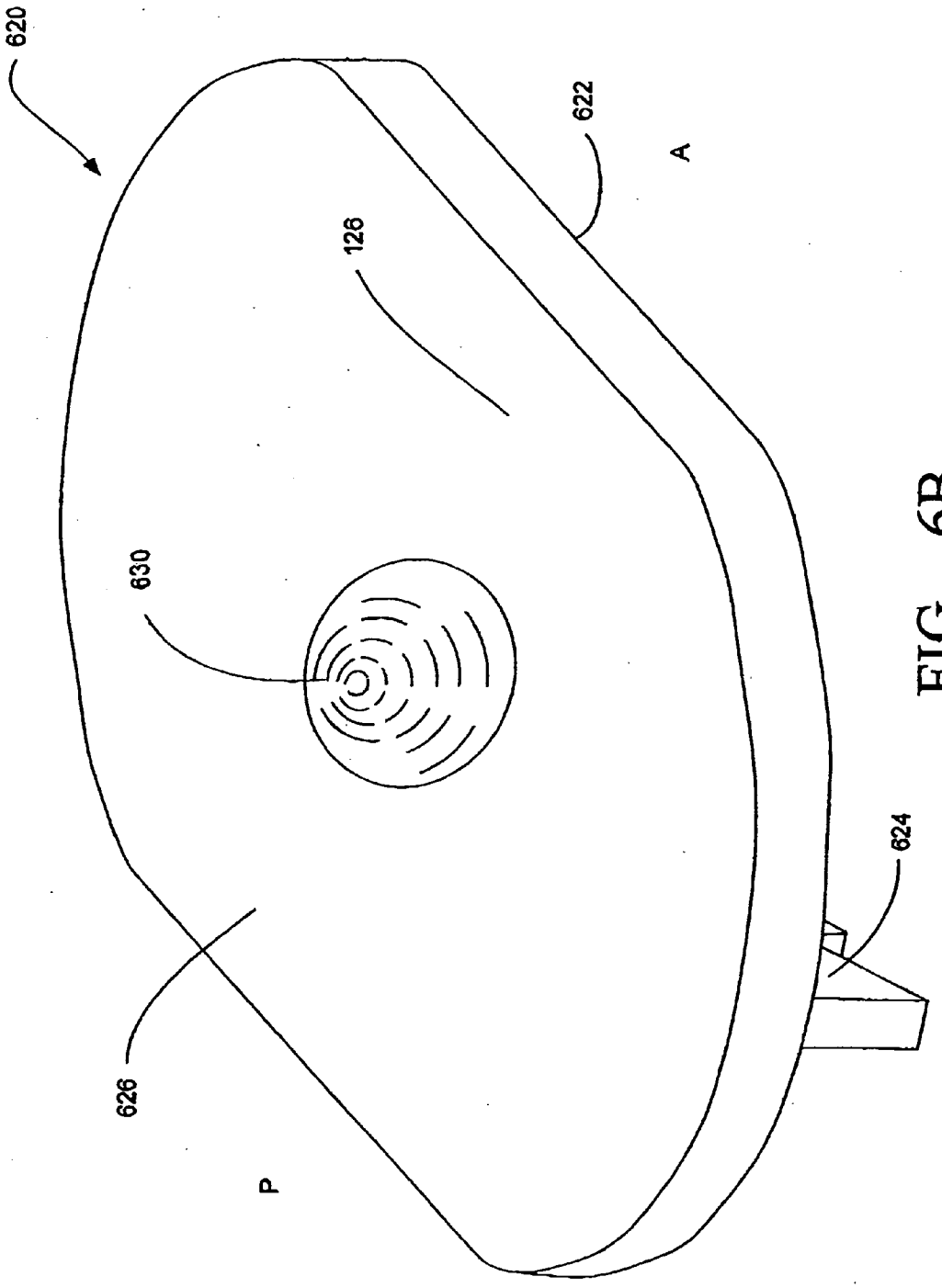


FIG. - 6B

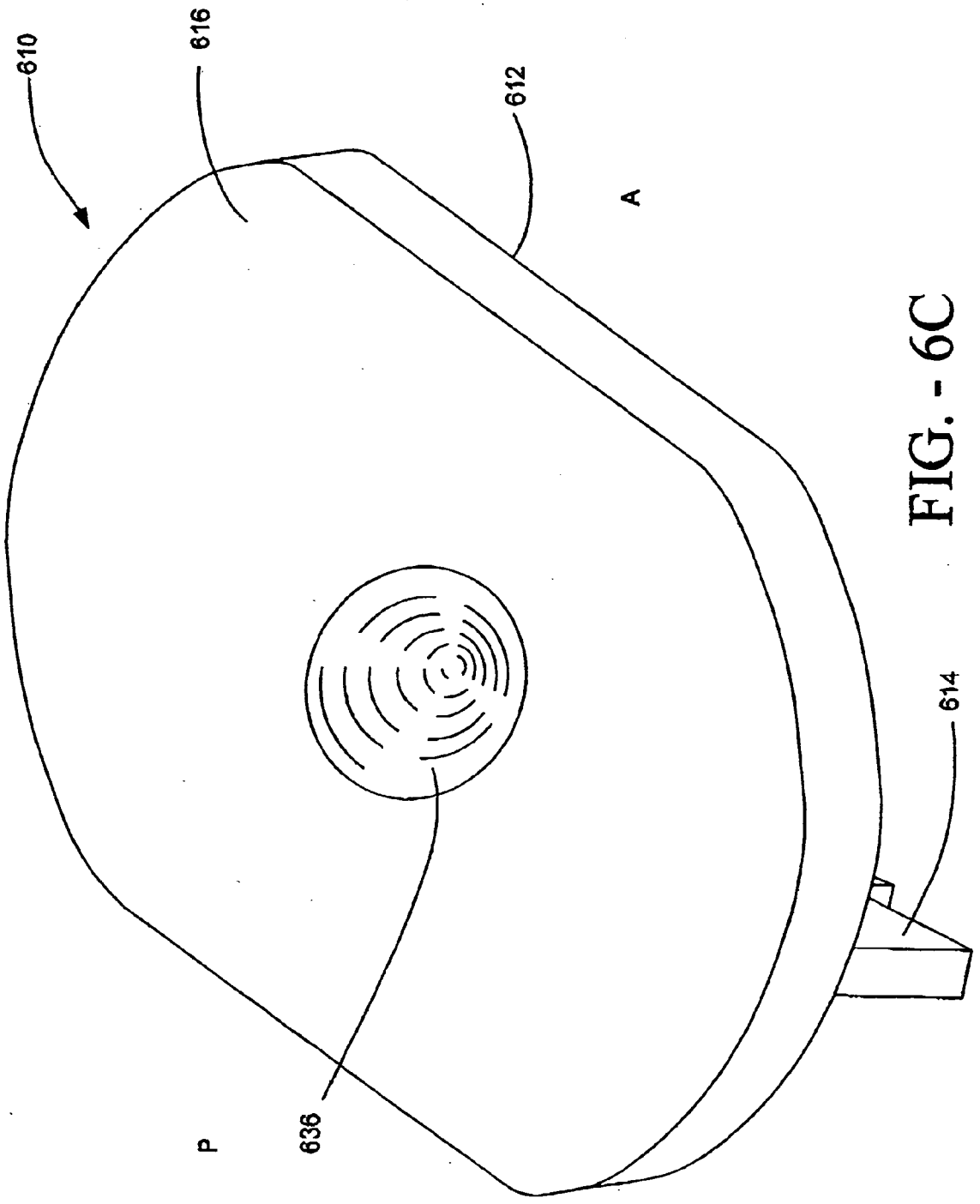


FIG. - 6C

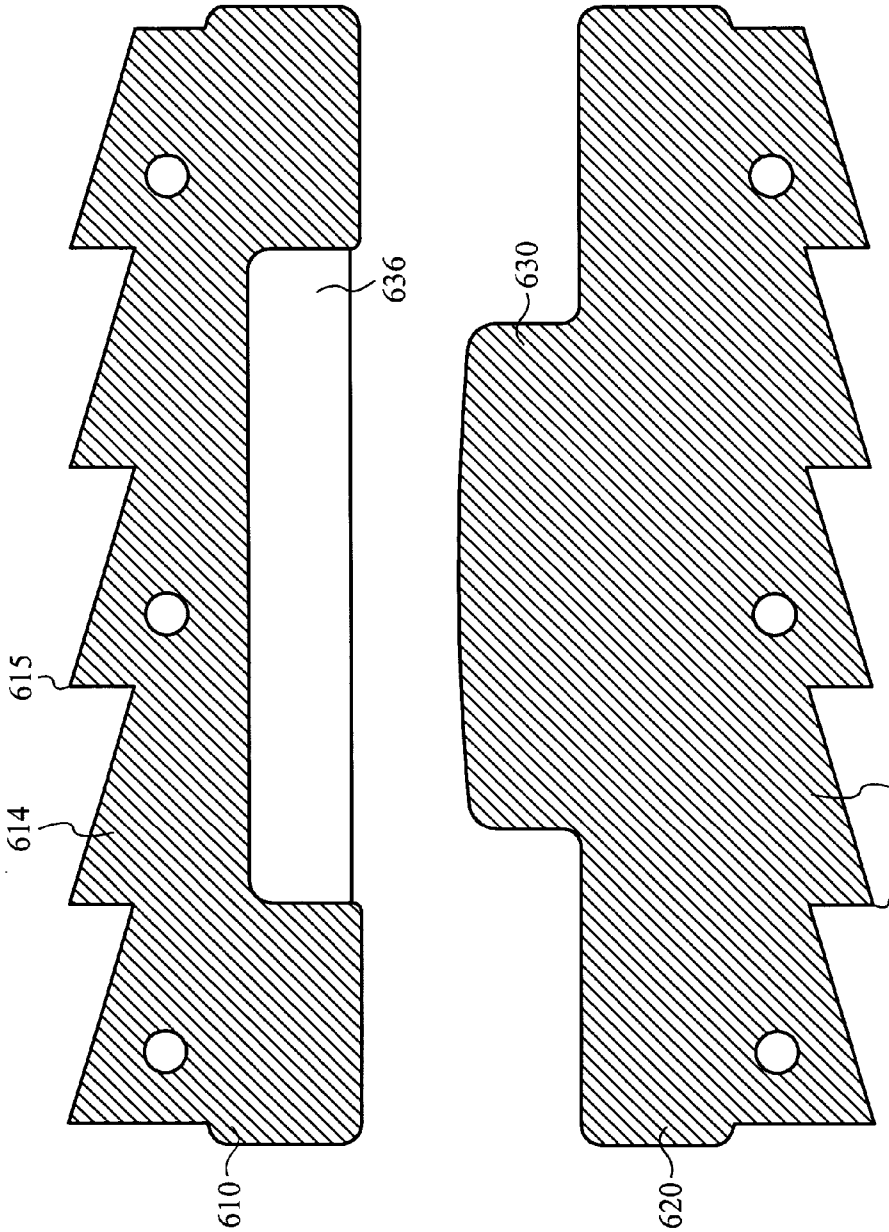


FIG. - 6D

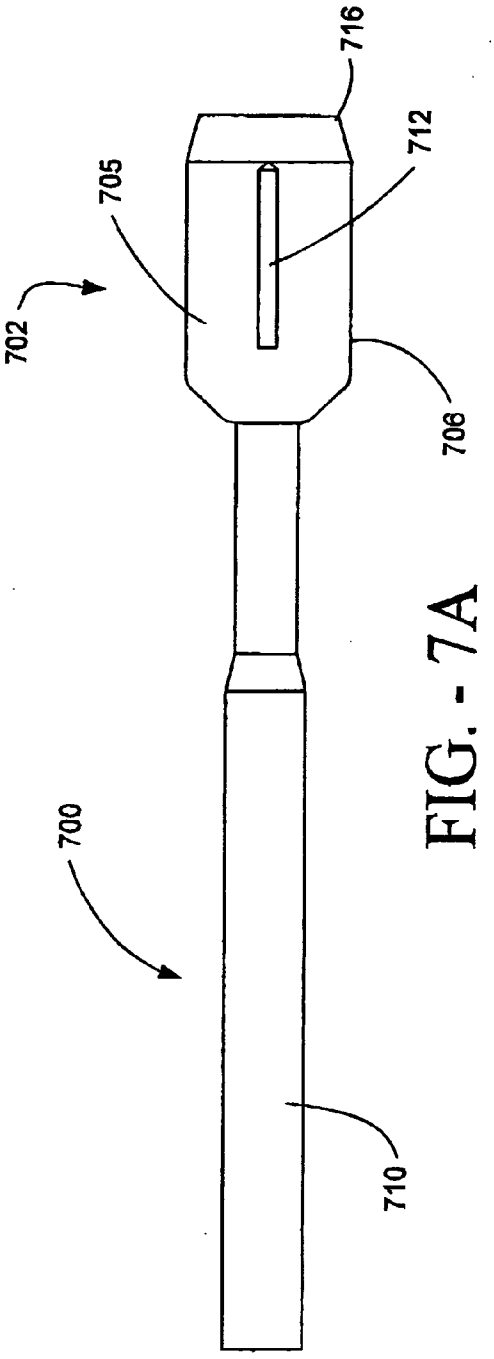


FIG. - 7A

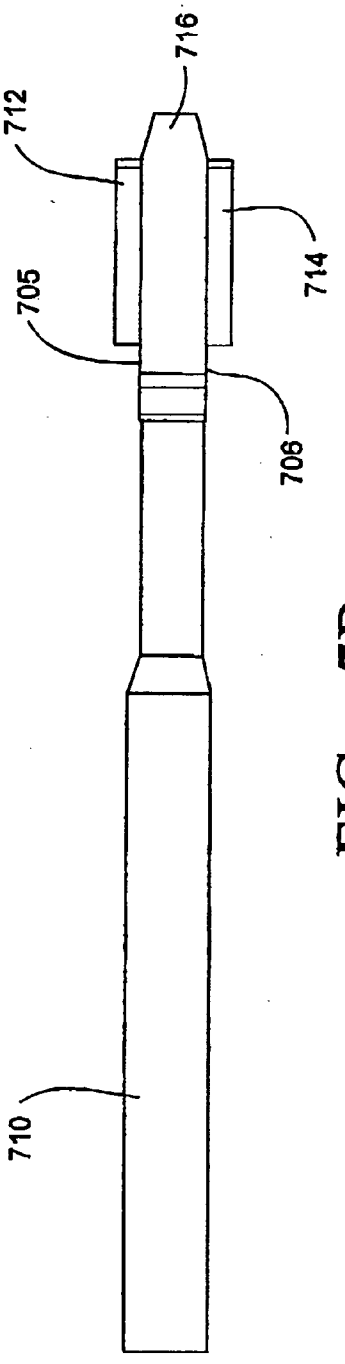


FIG. - 7B

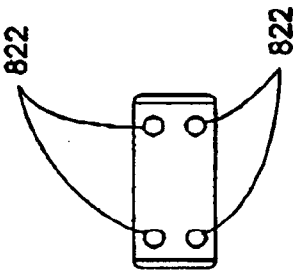


FIG. - 8C

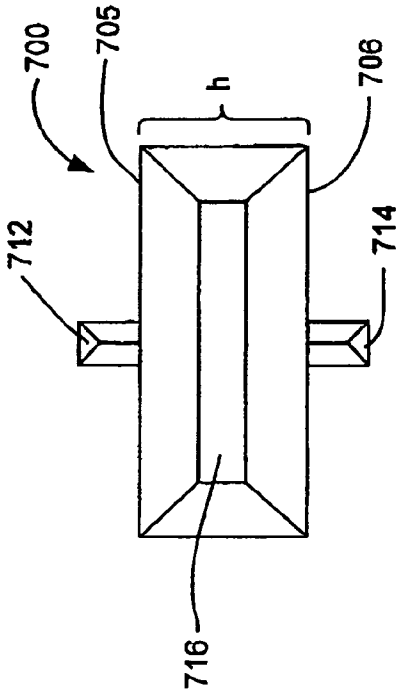


FIG. - 7C

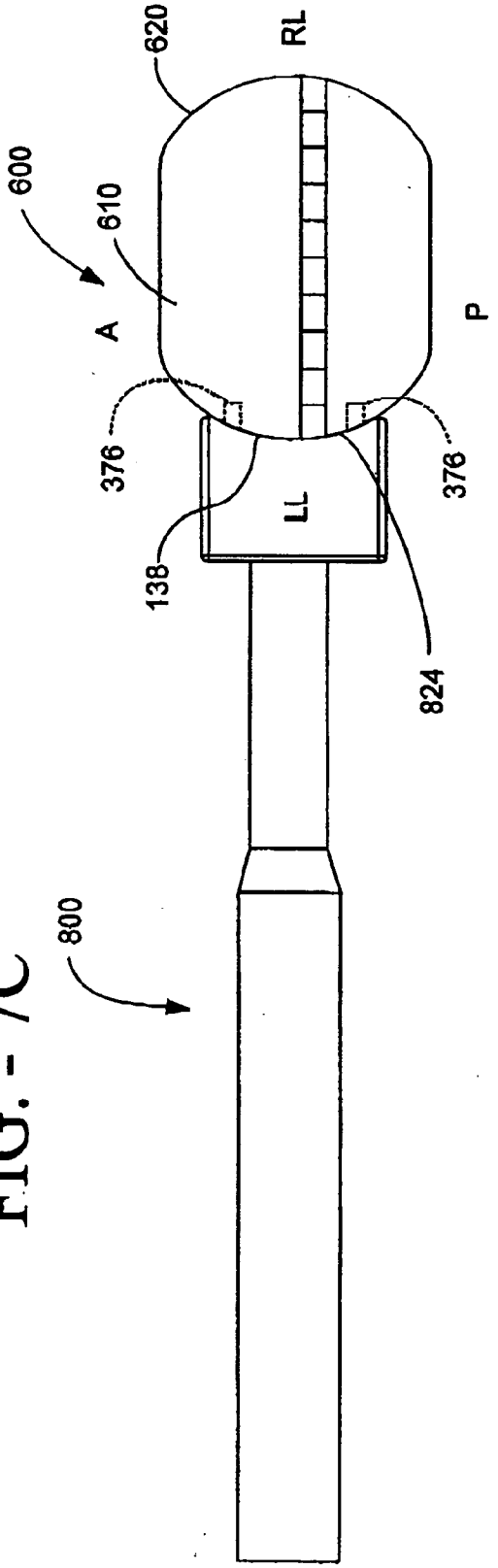


FIG. - 8D

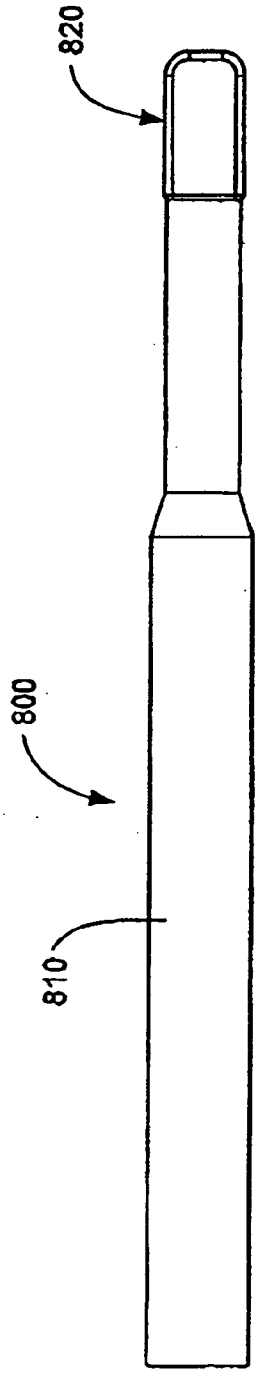


FIG. - 8A

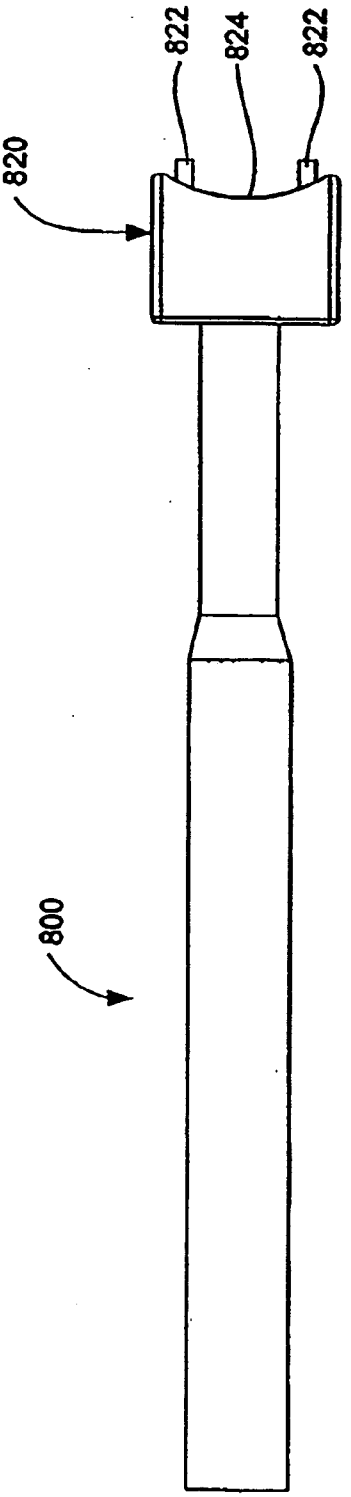


FIG. - 8B

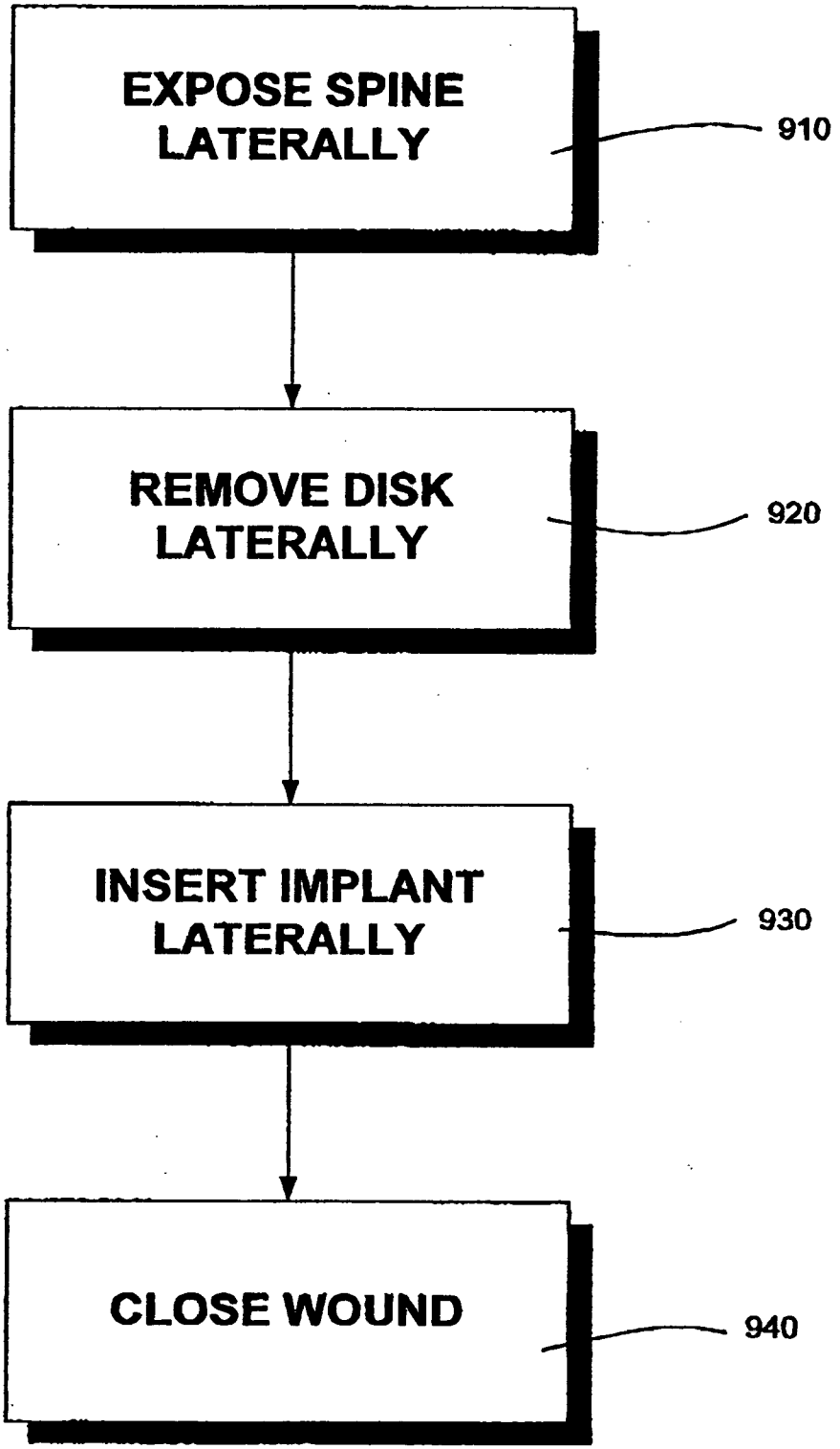

EXPOSE SPINE LATERALLY
910
REMOVE DISK LATERALLY
920
INSERT IMPLANT LATERALLY
930
CLOSE WOUND
940

FIG. - 9

LATERALLY INSERTABLE ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH TRANSLATING PIVOT POINT

CLAIM OF PRIORITY

[0001] This application claims priority under 35 USC 119 to U.S. Patent Application No. 60/526,724, filed on Dec. 2, 2003 and entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH TRANSLATING PIVOT POINT AND LATERAL IMPLANT METHOD," which is hereby incorporated by reference.

CROSS-REFERENCE TO RELATED APPLICATIONS

[0002] This application is related to U.S. Provisional Application No. 60/422,039, filed Oct. 29, 2002, entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH TRANSLATING PIVOT POINT AND METHOD," U.S. patent application Ser. No. 10/684,668, filed Oct. 14, 2003, entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH CROSSBAR SPACER AND METHOD," U.S. patent application Ser. No. 10/684,669, filed Oct. 14, 2003, entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH TRANSLATING PIVOT POINT AND METHOD," U.S. Provisional Application No. 60/422,011, filed Oct. 29, 2002, entitled "TOOLS FOR IMPLANTING AN ARTIFICIAL VERTEBRAL DISK AND METHOD," U.S. patent application Ser. No. 10/685,134, filed Oct. 14, 2003, entitled "TOOLS FOR IMPLANTING AN ARTIFICIAL VERTEBRAL DISK AND METHOD," U.S. Provisional Application No. 60/422,022, filed Oct. 29, 2002, entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH A SPACER AND METHOD," U.S. Provisional Application No. 60/422,021, filed Oct. 29, 2002, entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH CROSSBAR SPACER AND METHOD," U.S. patent application Ser. No. 10/685,011, filed Oct. 14, 2003, entitled "ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH SPACER AND METHOD," U.S. patent application Ser. No. _____, filed _____, entitled "METHOD OF LATERALLY INSERTING AN ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH TRANSLATING PIVOT POINT," (KLYCD-05007US6), U.S. patent application Ser. No. _____, filed _____, entitled "LATERALLY INSERTABLE ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH A CROSSBAR SPACER," (KLYCD-05008US6), U.S. patent application Ser. No. _____, filed _____, entitled "METHOD OF LATERALLY INSERTING AN ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH A CROSSBAR SPACER," (KLYCD-05008US7), U.S. patent application Ser. No. _____, filed _____, entitled "LATERALLY INSERTABLE ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH A SPACER," (KLYCD-05010US4), U.S. patent application Ser. No. _____, filed _____, entitled "METHOD OF LATERALLY INSERTING AN ARTIFICIAL VERTEBRAL DISK REPLACEMENT IMPLANT WITH A SPACER," (KLYCD-05010US5), all of which are incorporated herein by reference.

FIELD OF ART

[0003] This field of art of this disclosure is directed to an artificial vertebral disk replacement and method.

BACKGROUND

[0004] The spinal column is a biomechanical structure composed primarily of ligaments, muscles, vertebrae and intervertebral disks. The biomechanical functions of the spine include: (1) support of the body, which involves the transfer of the weight and the bending movements of the head, trunk and arms to the pelvis and legs, (2) complex physiological motion between these parts, and (3) protection of the spinal cord and nerve roots.

[0005] As the present society ages, it is anticipated that there will be an increase in adverse spinal conditions which are characteristic of aging. For example, with aging comes an increase in spinal stenosis (including, but not limited to, central canal and lateral stenosis), and facet joint degeneration. Spinal stenosis typically results from the thickening of the bones that make up the spinal column and is characterized by a reduction in the available space for the passage of blood vessels and nerves. Facet joint degeneration results from the constant load borne by the facet joints, and the eventual wear that results. Pain associated with both conditions can be relieved by medication and/or surgery.

[0006] In addition, to spinal stenosis, and facet joint degeneration, the incidence of damage to the intervertebral disks is also common. The primary purpose of the intervertebral disk is to act as a shock absorber. The disk is constructed of an inner gel-like structure, the nucleus pulposus (the nucleus), and an outer rigid structure comprised of collagen fibers, the annulus fibrosus (the annulus). At birth, the disk is 80% water, and then gradually diminishes with time, becoming stiff. With age, disks may degenerate, and bulge, thin, herniate, or ossify. Additionally, damage to disks may occur as a result disease, trauma or injury to the spine.

[0007] The damage to disks may call for a range of restorative procedures. If the damage is not extensive, repair may be indicated, while extensive damage may indicate full replacement. Regarding the evolution of restoration of damage to intervertebral disks, rigid fixation procedures resulting in fusion are still the most commonly performed surgical intervention. However, trends suggest a move away from such procedures. Currently, areas evolving to address the shortcomings of fusion for remediation of disk damage include technologies and procedures that preserve or repair the annulus, that replace or repair the nucleus, and that advance implants for total disk replacement. The trend away from fusion is driven both by issues concerning the quality of life for those suffering from damaged intervertebral disks, as well as responsible health care management. These issues drive the desire for procedures that are minimally invasive, can be tolerated by patients of all ages, especially seniors, and can be performed preferably on an out patient basis.

[0008] Most recently, there has been an increased interest in total disk replacement technology. A number of artificial disks are beginning to appear in the medical device marketplace. These artificial disks vary greatly in shape, design and functionality. With these devices go tools and methods for insertion between vertebrae thereof.

[0009] Accordingly, there is a need in the art for innovation in technologies and methods that advance the art in the area of minimally invasive intervertebral disk replacement. This not only enhances the quality of life for those suffering from the condition, but is responsive to the current needs of health care management.

BRIEF DESCRIPTION OF THE DRAWINGS

[0010] **FIG. 1A** is a posterior view of an embodiment of the assembled implant of the invention. **FIG. 1B** is a cross-section of the device shown in **FIG. 1A**. **FIG. 1C** is a posterior view of two bottom plates of the implant of the embodiment of the invention. **FIGS. 1D and 1E** are posterior views of the embodiment of the implant of the invention shown in **FIG. 1A** illustrating the operation of the device in bending to the left and bending to the right, respectively.

[0011] **FIG. 2A** is a side view of the implant of **FIG. 1A** showing the implant in flexion. **FIG. 2B** is a side view of the implant showing the implant in extension. **FIG. 2C** is a partial cross-sectional view of a side view of the implant of an embodiment of the invention. **FIG. 2D** is a partial cross-sectional view of an alternative embodiment of the implant of the invention having a protuberance adjacent the socket.

[0012] **FIG. 3A** is a top view of a portion of an embodiment of the assembled implant of the invention. **FIG. 3B** is a top view of an embodiment of the implant of the invention showing a rotation to the right. **FIG. 3C** is a top view of an embodiment of the implant of the invention showing a rotation to the left.

[0013] **FIG. 4A** and **FIG. 4B** show perspective views of the first and second inner surfaces of the first end plate and the second end plate of an embodiment of implant **100**.

[0014] **FIG. 5A** is a posterior view of the embodiment of the implant of the invention after being implanted between two vertebral bodies. **FIG. 5B** is a side view of the embodiment of the implant of the invention after being implanted between two vertebral bodies.

[0015] **FIG. 6A** is a rear view of an alternate embodiment of the invention having two plates. **FIG. 6B** and **FIG. 6C** show perspective views of the first and second inner surfaces of the first end plate and the second end plate of an alternative embodiment of implant **600**. **FIG. 6D** is a cross sectional view of the embodiment shown in **FIG. 6A**.

[0016] **FIG. 7A** is a top view of an embodiment of a cutting tool of the invention used to prepare the vertebral bodies for the implant. **FIG. 7B** is a side view of the embodiment of the cutting tool of the invention from the distal end. **FIG. 7C** is a distal end view of an embodiment of the cutting tool of the invention.

[0017] **FIG. 8A** is a side view of an embodiment of the implant lateral insertion tool of the invention. **FIG. 8B** is a top view of the embodiment of the implant lateral insertion tool of the invention. **FIG. 8C** is a distal end view of the embodiment of the implant lateral insertion tool of the invention. **FIG. 8D** is a top view of an embodiment of the implant lateral insertion tool holding an embodiment of the implant.

[0018] **FIG. 9** is a block diagram illustrating the steps of a method for inserting the implant between vertebral bodies.

DETAILED DESCRIPTION

[0019] The following description is presented to enable any person skilled in the art to make and use what is disclosed. Various modifications to the embodiments described will be readily apparent to those skilled in the art, and the principles defined herein can be applied to other embodiments and applications without departing from the spirit and scope of what is disclosed and defined by the appended claims. Thus, what is disclosed is not intended to be limited to the embodiments shown, but is to be accorded the widest scope consistent with the principles and features disclosed herein. To the extent necessary to achieve a complete understanding of what is disclosed herein, the specification and drawings of all patents and patent applications cited in this application are incorporated herein by reference.

[0020] **FIG. 1A** shows an embodiment of the implant **100** having a four-piece configuration. The designations, "A" for anterior, "P" for posterior, "RL" for right lateral, and "LL" for left lateral are given in the drawings for spatial orientation. These designations give the relationship of all faces of embodiments of the disclosed intervertebral implant from the superior perspective; i.e. looking down the axis of the spine. The implant **100** has a pair **131** of first end plates, or upper end plates **110** that are configured to mate with a first vertebra. The upper end plate **110** of implant **100** has a first outer surface **112** from which a first keel **114** extends with a first set of teeth **115**. Additionally, the implant **100** has a pair **133** of second end plates, or lower end plates **120** that are configured to mate with a second vertebra. The lower end plate **120** has a second outer surface **122** from which a keel **124** extends with a second set of teeth **125**. A pair of pivoting or articulating elements or spacers **130** that are part of the pair **133** of lower end plates **120** acts as an articulating element, or spacer between the first end plate **110** and the second end plate **120** and facilitates pivotal or rotational and also twisting movement of the first end plate **110** and the second end plate **120**, relative to each other. In the embodiments described, the pair of articulating elements, or spacers **130** is curved or convex, as will be discussed in more detail below.

[0021] Several configurations of implant **100** are contemplated. For instance, **FIG. 6A** illustrates a posterior view of an alternate embodiment of the implant shown in **FIG. 1A**. The implant **600** of **FIG. 6A** is in the form of a two-piece implant **600** having a first end plate **610** and a second end plate **620**. The first end plate, or upper end plate **610** is configured to mate with a first vertebra, and a second end plate, or lower end plate **620** is configured to mate with a second vertebra. The first inner surface **616** of the upper end plate **610** has a socket or first cavity **636** formed therein. A pivoting or articulation element, or spacer **630** is formed on second end plate **620**. The spacer **630** at least partially engages the first socket **636**, and facilitates pivotal or rotational and also twisting movement of the first end plate **610** and the second end plate **620**, relative to each other. The spacer **630** and corresponding socket **636** are dimensioned so that they are hemi-cylindrical (**FIG. 6D**), while in another embodiment shown in **FIG. 6B** and **FIG. 6C**, the articulating element, or spacer **630** and corresponding socket **636** are hemispherical.

[0022] The upper end plate **610** of implant **600** has a first outer surface **612** from which a first keel **614** extends with

a first set of teeth **615**. In one embodiment, when implant **600** is inserted between vertebrae, the first keel **614** extends longitudinally across the first outer surface **612**, about perpendicular to the sagittal plane of the spine. In another embodiment, the first keel **614** extends longitudinally only partially across the first outer surface **612**, about perpendicular to the sagittal plane of the spine. The teeth **615** in the two embodiments with complete or partial extension of the keel **614** across the first outer surface **612** of the upper end plate **610** point towards the left lateral face of implant **600** when the embodiment is meant to be put into a slot in a vertebral body from the left lateral approach to the spine. This orientation is shown in the figures, and is particularly evident where the keel **614** is fully displayed, as in **FIG. 1A** and **FIG. 6A**, for example. Alternatively, the teeth **615** point towards the right lateral face of implant **600** when the embodiments are meant to be put into a slot in a vertebral body from the right lateral approach to the spine.

[**0023**] The first outer surface **612** abuts the vertebral body when the implant **600** is implanted. The first keel **614** extends into the vertebral body to anchor implant **600** into position, and is perpendicular to the median sagittal plane of the spine, in which extension and flexion occur. The first keel **614** in this orientation offers substantial stability during extension and flexion for the implant **600** inserted between the vertebrae of a patient. Additionally, the first keel **614** in this embodiment is preferably aligned with and supports the articulation of implant **600**. The first inner surface **616** with socket **636** at least partially engages the spacer **630** of the implant and opposes the second end plate **620**. The first inner surface **616** can form a planar surface that is parallel to the first outer surface **612**, or can form a planar surface that is not parallel to the first outer surface **612**.

[**0024**] The lower end plate **620** has a second outer surface **622** from which a keel **624** extends with a second set of teeth **625**. In one embodiment, when implant **600** is inserted between vertebrae, the second keel **624** is about perpendicular to the sagittal plane of the spine. As described above for the first upper end plate **610**, in one embodiment, the second keel **624** extends longitudinally across the second outer surface **622**, while in another embodiment, the second keel **624** extends longitudinally partially across the second outer surface **622**. The teeth **625** in the two embodiments with complete or partial extension of the second keel **624** across the second outer surface **622** of the lower end plate **620** point towards the left lateral face of implant **600** when the embodiment is meant to be put into a slot in a vertebral body from the left lateral approach to the spine. This orientation is shown in the figures, and is particularly evident where the second keel **624** is fully displayed, as in **FIG. 1A** and **FIG. 6A**, for example. Alternatively, the teeth **625** point towards the right lateral face of implant **600** when the embodiments are meant to be put into a slot in a vertebral body from the right lateral approach to the spine.

[**0025**] The second outer surface **622** abuts the vertebral body when the implant **600** is implanted. The second keel **624** extends into the vertebral body to anchor implant **600** into position, and is perpendicular to the median sagittal plane of the spine, in which extension and flexion occur. The second keel **624** in this orientation offers substantial stability during extension and flexion for the implant **600** inserted between the vertebrae of a patient. Additionally, the second keel **624** in this embodiment is aligned with and supports the articulation of implant **600**. The second end plate **620** with second inner surface **626** having the spacer **630** opposes the first end plate **610** with first inner surface **616** having socket **636**. The spacer **630** of second inner surface **626** at least partially engages socket **636** of first upper surface. The second inner surface **626** can form a planar surface that is parallel to the second outer surface **622**, or can form a planar surface that is not parallel to the second outer surface **622**.

[**0026**] The first inner surface **616** of the first end plate **610** can be parallel to the second inner surface **626** of the second end plate **620** when the implant **600** is assembled and is in a neutral position (i.e., the position where the first end plate **610** has not rotated relative to the second end plate **620**). Alternatively, the first inner surface **616** of the first end plate **610** can be non-parallel to the planar surface of the second inner surface **626** of the second end plate **620** when the implant **600** is assembled and in a neutral position. This non-parallel orientation of the first end plate **610** and the second end plate **620** allows the plates to pivot to a greater degree with respect to each other. Additionally, factors such as the height and position of the spacer **630**, and the, can also be adjusted in order to increase the degree that the first end plate **610** and the second end plate **620** can pivot relative to each other. Other factors that effect the degree of movement of the first end plates **110** or **610** relative to the second end plates **120** or **620** for implant **100** or implant **600** will discussed below.

[**0027**] When implant **600** is inserted between vertebrae the planar surfaces corresponding to the first and second outer surfaces **612**, **622** and the first and second inner surfaces **616**, **626** of the first and second end plates **610**, **620** lie within, or substantially within, the axial plane of the body. Similarly, the first and second keels **614**, **624** are aligned in the axial plane, or perpendicular to the sagittal plane of the vertebrae. The first and second keels **614**,**624** extend into the vertebral bodies to anchor implant **600** into position, and are perpendicular to the median sagittal plane of the spine, in which extension and flexion occur. The first and second keels **614**,**624** in this orientation offer substantial stability during extension and flexion for implant **600** inserted between the vertebrae of a patient. Additionally, the first and second keels **614**,**624** in this embodiment are aligned with and support the axis of articulation of implant **600** defined by an RL to LL orientation.

[**0028**] The lateral orientation of the keels allow the implants to be inserted into the spine using a lateral approach as opposed to an anterior or posterior approach. The lateral approach is advantageous, because the spinal nerves in the spinal cavity are minimally undisturbed when the implants are inserted laterally into the spine. In comparison to a posterior insertion approach in which the spinal nerves can be substantially disturbed, the spinal nerves are bypassed and relatively undisturbed when the implant is inserted laterally between the vertebral bodies from the side of the spine. Although an anterior insertion approach has its benefits, the lateral insertion approach can allow the present implant and associated implantation tools, to be inserted into the spine with less disturbance of the patient's internal organs. This can translate into less time and risk associated with preparing the spine for insertion as well as inserting the implant itself into the spine. Further, the laterally oriented keels offer substantial stability to the vertebral bodies during extension, flexion and lateral bending of the spine.

[0029] In the embodiment shown in **FIG. 1A** and **FIG. 6A**, the first and second keels **114,124** and **614,624** include ports **148,152** and **648,652**, respectively, that facilitate bone ingrowth. For example, bone from the vertebral bodies can grow thorough the ports **148,152** and **648,652**, and aid in securing the first and second keels **114,124** and **614,624**, and thereby for securing implants **100** and **600** once inserted between vertebral bodies. In addition, surfaces defined by the first and second keels **114,124** and **614,624** and the first and second outer surfaces **112,122** and **612, 622** of implants **100** and **600** can be roughened in order to promote bone ingrowth into these defined surfaces of implants **100** and **600**. In other embodiments the ports **148,152** and **648,652**, the first and second keels **114,124** and **614,624**, and the first and second outer surfaces **112,122** and **612, 622** of implant **600** can be coated with materials that promote bone growth such as for example bone morphogenic protein, BMP, or structural materials such as hyaluronic acid, HA, or other substance which promotes growth of bone relative to and into the keels **614,624**, keel ports **648,652**, and other external surfaces of the implant **600**.

[0030] Further, a combination of the two embodiments shown in **FIG. 1A** and **FIG. 6A** can be used to create a three-piece implant as will also be appreciated by those of ordinary skill in the art. For example, the first end plate **610** of **FIG. 6A** with its socket **636** from a two-piece embodiment can be combined with two second end plates **120** of **FIG. 1A** from a four-piece embodiment to form an implant. Similarly, the second end plate **620** with spacer **630** of a two piece embodiment, such as **FIG. 6A**, can be combined with two first end plates **110** from a four-piece design, such as **FIG. 1A**, to achieve an implant. The features described herein for an interspinous implant for lateral insertion between adjacent vertebrae are applicable to two-, three-, or four-piece embodiments. None of these configurations depart from the scope of the invention.

[0031] **FIG. 1B** depicts the pair **131** of first or upper end plates **110** and the pair **133** of second or lower end plates **120** in cross-section. Each upper and lower end plate **110,120** has a keel **114,124** with a set of teeth **115,125**. As for implant **600**, different embodiments of implant **100** may have complete or partial extension of the first and second keels **114,124** across the first and second outer surfaces **112,122** of the upper and lower end plates **110,120**. The teeth **115,125** point towards the left lateral face of implant **100** when the embodiment is meant to be put into a slot in a vertebral body from the left lateral approach to the spine, and alternatively, the teeth **115,125** point towards the right lateral face of implant **100** when the embodiments are meant to be put into a slot in a vertebral body from the right lateral approach to the spine.

[0032] In **FIG. 1B**, the socket **136** formed in the first inner surface **116** of first end plate **110** has a first elongated sidewall **150**, a corresponding second elongated sidewall **152** (shown in **FIG. 3B**), an end wall **154**, and an open end **156**. The open ends **156** of each of the first end plates **110** are oriented so that the open ends **156** face each other. Each of the first and second end plates **110, 120** has a first end **138, 141** and a second end **139, 143**. The ends **139** of the first end plate **110** face each other, as do the ends **143** of the second end plate **120**. The lower plates **120** each have an articulating element, or spacer **130**, which is convex and hemi-cylindrical, that engage the socket **136**. The concave hemi-cylindrical inner surface **135** of the socket **136** is sloped to allow the pair **131** of first or upper end plates **110** to easily slide, or rock, side-to-side on the articulating element, or spacer **130** and slide, or ride, forward and backward with enough looseness of fit to allow for some twisting in order to emulate the motion of the vertebral bone and intervertebral disk tissue. This arrangement, thus, has a sliding or translating pivot point. It is evident from **FIG. 1B** that the first and second keels **114,124** are aligned with and support the axis of articulation of the upper end plate **110** about the spacer **130** for this embodiment. This axis of articulation is longitudinally oriented with respect to the vertebrae, or about perpendicular to the sagittal plane of the spine. The alignment of the first and second keels **114,124** with the axis of articulation offers substantial stability during flexion and extension when implant **100** is inserted between the vertebrae of a patient.

[0033] As shown in **FIG. 1C**, the articulating element, or spacer **130** has four sides: a first elongated sidewall **140**, a second elongated sidewall **142**, a third end wall **143**, and a fourth end wall **146**. The third end wall **144** is flush with the end **143** of the lower end plate **120** of the implant. The third end wall **144** has a profile height **160** and the fourth end wall **146** has a profile height **162**. Comparing the profile heights **160, 162** to each other at the same point on the second inner surface **126** of the second end plate **120**, the overall profile height of the third end wall **144** is greater than the fourth end wall **146** (i.e., **160**>162). Thus, it is evident that the upper surface **135** of socket **136** slopes downwardly from the end wall **144** to the end wall **146**. Together spacers **130** comprise an articulating element that has a high surface where the third end walls **144** abut each other and slope to a lower surface adjacent to fourth end walls **146**.

[0034] In **FIG. 1C**, the edges of the articulating element or spacer **130** are eased or rounded to allow for further range of motion of the pair **131** of upper end plates **110** relative to the pair **133** of lower end plates **120**. As will be appreciated by those of skill in the art, the overall height of the third end wall **144** and the fourth end wall **146** can be equivalent while still having an effective third end wall height **160** that is greater than the effective fourth end wall height **162** due to the overall slope of the second inner surface **126**. Alternatively, the overall height of the third end wall **144** and the fourth end wall **146**, can be different with the third end wall **144** having a height greater than the fourth end wall **146**, thus eliminating the need for the second inner surface **126** to have a slope or further increasing the net difference between the height of the third end wall and the forth end wall. Further, although the spacer **130** is depicted such that the third end wall **144** is flush with the second end **143**, those of skill in the art will appreciate that the spacer **130** could also be configured such that the third end wall **144** is recessed relative to the end **143** of the second end plate. In such a configuration, the third end wall **144** and the end **143** would not be flush.

[0035] **FIGS. 1D and 1E** illustrate posterior views of the implant **100** showing the clearance for left and right lateral bending. Typically, left and right lateral bending ranges from 3-5°. As evident from these figures, the length of the spacer **130** can be less than the length of the socket **136**. As shown, the open ends **156** of the sockets facilitate movement of the articulating elements, or spacers **130** within the socket **136** to accommodate side-bending movement.

[0036] **FIG. 2A** and **FIG. 2B** are views of the intervertebral implant **100**, which depict the motion of the first end plate **110** relative to the second end plate **120**. In **FIG. 2A** and **FIG. 2B**, a side view of implant **100** is depicted, showing first end plate **110** with socket **136** and the second end plate **120** with the articulating element or spacer **130**. As is apparent from the figures, the sloping of the first inner surface **116** of the first end plate **110** facilitates rotation of the spacer and socket in an anterior A direction and a posterior P direction. As depicted, the first inner surface **116** slopes from a high point at about where the socket is located to low points at the ends **111** and **113** of the upper end plate **110**. As shown in **FIG. 2A**, the implant **100** is positioned to achieve flexion (i.e., forward bending) in a range up to about 15°, but more preferably 10°, while in **FIG. 2B**, the implant **100** is positioned to achieve extension (i.e., backward bending) in a preferable range of up to about 5°.

[0037] **FIG. 2C** and **FIG. 2D** show cross sections of implant **100** through the sagittal plane of the vertebrae. **FIG. 2C** is a cross-section of the side view of the intervertebral implant **100** showing the mating of the spacer **130** to the socket **136**. **FIG. 2D** illustrates an alternate embodiment of the first end plate **110** wherein the socket **136** has ridges **268**, **269** forming a protuberance that extends into the channel **264**, **265** respectively on the second end plate **120**. As will be appreciated by those of skill in the art, the protuberances **268**, **269** can extend partially into the channel, such as the configuration shown, or can have a channel conforming shape such that when the spacer and socket are moved to achieve flexion **272** or extension **274** the protuberance or ridge **268**, **269** extends into the channels **264**, **265**. This embodiment allows the first inner surface **116** and second inner surface **126** of the first end plate **110** and the second end plate **120** to be flat and non-sloping as shown while still allowing for the implant to emulate forward and backward bending and allow for the blocking of the motion of the socket relative to the spacer. In this embodiment, it is noted that the first and second keels **114**,**124** are aligned with and support the articulation of first end plate **110** about the spacer **130** for this embodiment, and where the articulation is about perpendicular to the sagittal plane of the spine.

[0038] Turning now to **FIG. 3A**, a top view of one-half of the intervertebral implant **100** is shown. Each of the top first end plate **110** and the bottom second end plate **120** have a bores **376** for receiving pins of an implant tool. The first keel **114** on the first end plate **110** is positioned so that it is aligned in the same plane with the second keel **124** on the second end plate **120**. Additionally, the length of spacer **130** from the third end wall **144** to the fourth end wall **146** is shorter than the length of the socket **136** from the end wall **154** to the open end **156**, so that the fit of the spacer with the socket is somewhat loose. The loose fit of the spacer **130** in the socket **136** allows the first end plate **110** to be able to twist somewhat relative to the second plate **120**. This twisting action would generally be about an axis that is perpendicular to the first and second inner surfaces **116**,**126** of the first and second end plates **110**,**120**, respectively. Thus, implant **100** of this embodiment allows the spine to have movement in three orthogonal degrees of freedom, namely (1) forward and backward bending movement, (2) lateral side-to-side bending, and (3) twisting movement. **FIGS. 3B and 3C** show the relative rotation of the first or upper end plate **110** to the second or lower end plate **120** to achieve rotation about a central axis **378**. This rotation results in about a 3°-6° rotation about the axis (i.e., 3° of torso twisting in each direction).

[0039] **FIG. 4A** and **FIG. 4B** show views of the first and second end plates, **110**,**120**. **FIG. 4A** shows a perspective view of a second end plate **120** of the intervertebral implant **100**. The second inner surface **126** of the second end plate **120** is shown with a hemi-cylindrical spacer **130** formed therefrom, and channels or grooves **264**, **265** extending about the spacer **130**. As illustrated in **FIG. 4A**, the channels **264**, **265** are formed on two sides of the spacer **130**. However, as will be appreciated by those of skill in the art, the channels **264**, **265** can alternatively surround the spacer **130**. The channels allow the sides of the spacer **130** to be made more perpendicular so as to create a greater blocking wall thus preventing the socket of the upper plate **100** from moving too much anteriorly or posteriorly relative to the lower plate **120**. **FIG. 4B** shows a perspective view of the first end plate **110**, with a first inner surface **116** that opposes the second inner surface **126**. The first inner surface **116** has a hemi-cylindrical socket **136** formed therein. The socket **136** of **FIG. 4B** is configured to mate with the spacer **130** of **FIG. 4A**.

[0040] **FIG. 4***c* and **FIG. 4***d* show views of the first and second end plates, **110**, **120** for an alternative embodiment of implant **100**. **FIG. 4***c* shows a perspective view of an embodiment of the second inner surface **126** of the second or lower end plate **120** of implant **100**. The second inner surface **126** of the lower end plate **120** has a hemispherical spacer **130** formed therefrom. **FIG. 4***d* shows a perspective view of an embodiment of the first inner surface **116** of the first or upper end plate **110** of implant **100**, which opposes the second inner surface **126**. The first inner surface **116** of the upper end plate **110** has a socket or cavity **136** formed therein. In the embodiment of **FIG. 4***d*, the socket **136** has a concave hemispherical surface. The socket **136** allows the first end plate **110** to pivot or rotate on spacer **130**.

[0041] In the embodiments shown in **FIG. 4A** and **FIG. 4B**, it is noted that the first and second keels **114**,**124** are aligned with and support the articulation of the first end plate **110** about the spacer **130**, relative to the second end plate **120**. The first and second keels **114**,**124** in this orientation offer substantial stability during extension and flexion for implant **100** inserted between the vertebrae of a patient. Additionally, the first and second keels **114**,**124** in these embodiments are aligned with and support the lateral axis of articulation of implant **100**, which is perpendicular to the sagittal plane of the spine. Additionally, as evidenced from the perspective views of **FIG. 4A** and **FIG. 4B**, the perimeter shape of the upper and lower end plates **110**,**120** can be configured to correspond to the perimeter shape of a vertebral disk. As will be appreciated by those of ordinary skill in the art, the perimeter shape of the upper end plate **110** and the lower end plate **120** can be the same.

[0042] **FIG. 5A** and **FIG. 5B** show the implant after insertion between the vertebrae of a patient. **FIG. 5A** illustrates a posterior view of the implant shown in **FIG. 1A** implanted between vertebral bodies in a spine. **FIG. 5A** illustrates the spinal column **500** and the cauda equina **504** (a collection of lumbar and sacral nerve roots that fill the caudal end of the spinal cord) with individual nerves **506** exiting the cord between lumbar vertebrae. The implant **100** is positioned between two vertebral bodies **520**, **521** such

that the first and second keels **114**, **124** lie in a plane parallel to coronal or frontal plane of the body, or perpendicular to the sagittal plane of the vertebrae. **FIG. 5B** illustrates a side view of the implant inserted between vertebral bodies **520**, **521**, for embodiments of the implant as that shown in **FIG. 1A**, or **FIG. 6A**. The gap between the first end plate **110** and the second end plate **120** at the anterior "A" face of implants **100**,**600** is greater than at the posterior "P" face of implants **100**,**600**. The greater gap at the anterior face vs. the posterior face of implants **100**,**600** results in the flexion (forward bending) movement being facilitated to a greater degree than extension (backward bending) movement. Thus, for these embodiments, an example of a forward bending movement of up to 10° can be achieved while a backward bending movement of 5° will be achieved. These embodiments show implants **100**,**600** inserted between two vertebrae with two first keels **114** extending from the first end plate **110**, and two second keels **124** extending from the second end plate **120**. The first and second keels **114**,**124** are about perpendicular to the sagittal plane of the spine, and support the articulation of the first end plate **110** relative to the second end plate **120**, about the spacer **130**.

[**0043**] The embodiments of implants **100**, **600** can be made of medical grade titanium, stainless steel or cobalt chrome. Other materials that have appropriate structural strength and that are suitable for implantation into a patient can also be used.

[**0044**] One class of materials contemplated for use in implant **100** is the class of biocompatible polymers. Copolymers, blends and composites of polymers are also contemplated for fabrication of parts of the disclosed device. A copolymer is a polymer derived from more than one species of monomer. A polymer composite is a heterogeneous combination of two or more materials, wherein the constituents are not miscible, and therefore exhibit an interface between one another. A polymer blend is a macroscopically homogeneous mixture of two or more different species of polymer.

[**0045**] One group of biocompatible polymers are the polyaryl ester ketones which has several members, which include polyetheretherketone (PEEK), and polyetherketoneketone (PEKK). PEEK has proven as a durable material for implants, as well as meeting criteria of biocompatibility. Medical grade PEEK is available from Victrex Corporation under the product name PEEK-OPTIMA. Medical grade PEKK is available from Oxford Performance Materials under the name OXPEKK, and also from CoorsTek under the name BioPEKK. Still another interesting group of biocompatible polymers are polyalkyl biocompatible polymers, such as polyethylenes, polypropylenes, and the like.

[**0046**] These medical grade biocompatible polymers are also available as reinforced polymer materials. To reinforce a polymeric material, fillers, are added to a polymer, copolymer, polymer blend, or polymer composite. Fillers are added to modify properties, such as mechanical, optical, and thermal properties. In this case, fillers, such as carbon fibers, are added to reinforce the polymers mechanically to enhance strength for certain uses, such as load bearing devices.

[**0047**] In addition to disclosure of embodiments of an intervertebral implant, tools for preparing and inserting an intervertebral implant are also disclosed. **FIG. 7A through 7D** show an embodiment of a tool for preparing vertebral bodies to receive implants **100**,**600**, while **FIG. 8A** through **FIG. 8D** show an embodiment of a tool for inserting embodiments of the disclosed intervertebral implants **100**, **600**.

[**0048**] **FIG. 7A** through **FIG. 7C** are the top view, the side view, and an end view of the cutting tool **700**. The cutting tool **700** has a handle **710** at its proximal end for controlling the tool during operation. As will be appreciated by those of skill in the art, the handle **710** can be removable or affixed to the cutting end. The distal end **702** of the tool **700** is solid head has an upper surface **705**, and a lower surface **706**. The upper surface **705** has a first blade **712** mounted thereon, and the lower surface **706** has a second blade **714** mounted thereon. Preferably the first blade **712** is about centered with the upper surface **705**, and the second blade **714** is about centered with the lower surface **706**. The first and second blades **712**,**714** are oriented to cut a space in a first and second intervertebral body for the first and second keels **114**,**124** of implants **100**,**600**. The space is perpendicular to the sagittal plane of the vertebrae, and allows for the lateral insertion of the implants **100**,**600**. **FIG. 7C** is a view of the distal end of the cutting tool **700** showing the beveled end **716** and the first and second blades **712**,**714**. The height h of the head **702** of the cutting tool **700** approximates the distance between two vertebral bodies or the height of the disk space. In this embodiment of cutting tool **700**, the blades **712**, **714** extend above and below the head **702**.

[**0049**] As will be appreciated by those of skill in the art, the tool shown in **FIG. 7A** can be modified such that instead of cutting keel-receiving channels in the upper and lower vertebral bodies at the same time, two tools are provided so that only one vertebral body is cut for keel-receiving channels at a time. For example, an alternative embodiment of cutting tool **700** has a first tool with a single blade mounted on the head **702**. A second tool could be provided having a single blade mounted on the head **702**, and additionally on the opposing surface, a guide. The guide on the surface opposite the surface with the blade is designed to engage with the first keel receiving channel cut the first vertebrae with the first tool to ensure that the second cut is optimally aligned with the first cut.

[**0050**] **FIG. 8A** through **FIG. 8D** depict an embodiment of the implanting tool used to insert the implant **600** of **FIG. 6A** between vertebral bodies. **FIG. 8A** is a side view of the implantation tool **800** that has a handle **810** and an implant holder **820**. The implant holder **820** has an implant conforming surface **824** and four pins **822** for holding the first end plate **610** and the second end plate **620** implant **600**. The conforming surface **824** is curved to follow the convex outer LL edges of the first and second end plates **610**, **620**, respectively, for an implant inserted from the left lateral side of a patient. The implant **600** nests within a conforming surface **824** and is held by pins **822**. **FIG. 8C** shows the distal view of the end of the tool with four pins **822** for securing the first and second end plate of the implant.

[**0051**] A variety of kits can be assembled that include an implant **100** (or **600**) sized for a particular patient. The kit could also include several cutting tools **700** and several implanting tools **800** or a single handle that cooperates with cutting ends **702** and implantation ends **820**.

[**0052**] **FIG. 9** is a block diagram showing the basic steps of the method for laterally inserting the embodiments of

implants **100,600**. First the spine is exposed through a lateral access **910**, then the intervertebral disk is removed laterally **920**, if necessary. A tool, such as the one depicted in **FIG. 7A** is inserted laterally between the vertebral bodies to create channels in the bodies to receive the keels of the implant. The implant is then inserted laterally **930** between two vertebrae and the wound is closed **940**. This procedure can be followed for either a left lateral approach or right lateral approach. For a left lateral approach, the teeth **115**, **125** of upper and lower keels **114**, **124** would be pointed towards the left lateral face of the device in order to aid in retaining embodiments of implants **100,600** in place. For a right lateral approach, the teeth would point towards the right lateral face of the device.

[**0053**] What has been disclosed herein has been provided for the purposes of illustration and description. It is not intended to be exhaustive or to limit what is disclosed to the precise forms described. Many modifications and variations will be apparent to the practitioner skilled in the art. What is disclosed was chosen and described in order to best explain the principles and practical application of the embodiments described herein, thereby enabling others skilled in the art to understand the various embodiments and various modifications that are suited to the particular use contemplated. It is intended that the scope of what is disclosed be defined by the following claims and their equivalence.

What is claimed:

1. An intervertebral implant comprising:

a first end plate with a first inner surface;

a second end plate with a second inner surface opposing the first inner surface, where the second inner surface has an articulating element formed thereon; and

an attachment mechanism adapted to engage a vertebral body, wherein the attachment mechanism is adapted to extend, when implanted, along a lateral direction with respect to the vertebral body.

2. The implant of claim 1 wherein the articulating element allows movement of the vertebral body in between flexion to extension directions.

3. The implant of claim 1 wherein the attachment mechanism is aligned with and supports the articulating element.

4. The implant of claim 1 wherein the articulating element further comprises an elongated hemi-cylindrical structure protruding from the second inner surface and an elongated cavity in the first inner surface adapted to receive the hemi-cylindrical structure.

5. The implant of claim 1 wherein the attachment mechanism is a keel upstanding from at least one of the first end plate and the second end plate.

6. An intervertebral implant comprising:

a first end plate adapted to mate with a first vertebral body further comprising:

a first inner surface;

a first outer surface; and

at least one keel on the first outer surface, wherein the keel is adapted to be perpendicular to a sagittal plane of the first vertebral body when implanted thereto;

a second end plate adapted to mate with a second vertebral body further comprising;

a second inner surface opposing the first inner surface, wherein the second inner surface has a spacer coupled thereto; and

a second outer surface.

7. The implant of claim 6 wherein the spacer allows bending from flexion to extension.

8. The implant of claim 6, where the keel is aligned with and supports the spacer.

9. The implant of claim 6, further comprising at least one keel on the second outer surface, wherein the keel is oriented perpendicular to the sagittal plane when implanted to a second vertebral body.

10. The implant of claim 9 wherein the keel is supports the spacer.

11. An intervertebral implant comprising:

a first end plate adapted to mate with a first vertebral body further comprising:

a first inner surface;

a first outer surface; and

at least one keel on the first outer surface, where the keel is adapted to be perpendicular to the sagittal plane of the vertebrae when implanted thereto;

a second end plate adapted to mate a second vertebrae, comprising:

a second inner surface opposing the first inner surface, where the second inner surface has extending spacer therefrom;

a second outer surface; and

at least one keel on the second outer surface, where the keel is adapted to be perpendicular to the sagittal plane of the vertebral body when implanted thereto.

12. The intervertebral implant of claim 11 wherein the spacer allows bending from flexion to extension.

13. The intervertebral implant of claim 11 wherein the keels on the first outer surface and the second outer surface support the spacer.

14. The intervertebral implant of claim 11 wherein the first end plate and second end plate have a lateral dimension longer than an anterior-posterior dimension.

15. An interspinous disk replacement implant adatped to be inserted between adjacent vertebral bodies, the implant having a first end plate, a second end plate, and an articulating element formed on the second end plate, the improvement comprising the implant having at least one keel that is about perpendicular to the sagittal plane of a vertebral body.

16. The implant of claim 15 wherein the articulating element is hemi-cylindrical.

17. An interspinous disk replacement implant adapted to be inserted between adjacent vertebral bodies, the implant having an articulating unit with a first end plate having a first inner surface with a first socket therein, a second end plate having a second inner surface opposing the first inner surface, the second inner surface with an articulating element formed thereon, where the articulating element is at least partially received in the first socket, the improvement of the implant comprising the implant having at least one keel extending from the articulating unit that is about perpendicular to the sagittal plane of a vertebral body.

18. The implant of claim 17 wherein the articulating element is hemi-cylindrical.

19. An interspinous disk replacement implant having a first end plate, a second end plate, and an articulating element between formed on the second end plate, the improvement comprising the implant having an attachment mechanism that supports the articulating element, the attachment mechanism adapted to laterally engage an adjacent vertebrae.

20. The implant of claim 19 wherein the attachment mechanism is at least one keel.

21. The implant of claim 19 wherein the articulating element is hemi-cylindrical.

22. An interspinous disk replacement implant having an articulating unit with a first end plate having a first inner surface with a first socket therein, a second end plate having a second inner surface opposing the first inner surface, the second inner surface with an articulating element formed thereon, where the articulating element is at least partially received in the first socket, the improvement of the implant comprising the implant having an attachment mechanism is aligned with and supports the articulating element, the attachment mechanism adapted to laterally engage an adjacent vertebrae.

23. The implant of claim 22 wherein the attachment mechanism is at least one keel.

24. The implant of claim 22 wherein the articulating element is hemi-cylindrical.

25. A kit to insert an interspinous disk replacement implant in a spine, the kit comprising:

an interspinous disk replacement implant adapted for lateral insertion into the spine; and

at least one tool for preparing the spine to receive the implant.

26. An interspinious implant comprising:

a first end plate having a first anterior end, a first posterior end and two first lateral ends extending between the first anterior and posterior ends;

a second end plate having a second anterior end, a second posterior end and two second lateral ends extending between the second anterior and posterior ends;

a spacer extending from the second end plate, the spacer having an elongated hemi-cylindrical configuration;

a first keel protruding from a first outer surface of the first end plate, wherein the first keel is oriented lengthwise between the two first lateral ends; and

a second keel protruding from a second outer surface of the second end plate, wherein the second keel is oriented lengthweise between the two second lateral ends.

27. An interspinous implant adapted to be inserted between adjacent vertebral bodies comprising:

an implant body having a first outer surface adapted to mate with a first vertebral body and a second outer surface adapted to mate with a second vertebral body;

an articulating element within the implant body, the articulating element having an elongated spacer and corresponding elongated socket;

a first keel protruding from the first outer surface and oriented generally parallel to the articulating element.

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