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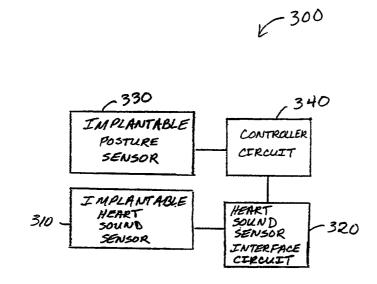
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(54) Title: DEVICE MEASURING HEART SOUNDS AND POSTURE



(57) Abstract: A system to monitor heart sounds. The system comprises an implantable heart sound sensor operable to produce an electrical signal representative of at least one heart sound, a heart sound sensor interface circuit coupled to the heart sound sensor to produce a heart sound signal, an implantable posture sensor operable to produce an electrical signal representative of a patient's posture, and a controller circuit, coupled to the heart sound sensor interface circuit and the posture circuit. The controller circuit is operable to measure at least one heart sound in correspondence with at least one sensed patient posture.

DEVICE MEASURING HEART SOUNDS AND POSTURE

Claim of Priority

Benefit of priority is hereby claimed to U.S. Patent Application Serial Number 11/037,275, filed on January 18, 2005, which application is herein incorporated by reference.

Cross-Reference to Related Applications

This application is related to the following co-pending, commonly assigned U.S. Patent Applications: Serial No. 10/900,570, entitled "DETERMINING A PATIENT'S POSTURE FROM MECHANICAL VIBRATIONS OF THE HEART," filed on July 28, 2004, Serial No. 10/703,175, entitled "A DUAL USE SENSOR FOR RATE RESPONSIVE PACING AND HEART SOUND MONITORING," filed on November 6, 2003, and Serial No. 10/334,694 entitled "METHOD AND APPARATUS FOR MONITORING OF DIASTOLIC HEMODYNAMICS," filed on December 30, 2002, which are hereby incorporated by reference.

Technical Field

The field generally relates to implantable medical devices and, in particular, but not by way of limitation, to systems and methods for monitoring the mechanical functions of the heart.

Background

Implantable medical devices (IMDs) are devices designed to be implanted into a patient. Some examples of these devices include cardiac rhythm management (CRM) devices such as implantable pacemakers, implantable cardioverter defibrillators (ICDs), and devices that include a combination of pacing and defibrillation. The devices are typically used to treat patients using electrical therapy and to aid a physician or caregiver in patient diagnosis through internal monitoring of a patient's condition. The devices may include electrical leads in communication with sense amplifiers to monitor electrical heart activity within a patient, and often include sensors to monitor other internal patient parameters. Other examples of implantable medical

devices include implantable insulin pumps or devices implanted to administer drugs to a patient.

Heart sounds are associated with mechanical activity of a patient's heart. The first heart sound (S1) is the sound made by the heart during the near simultaneous closure of the mitral and tricuspid valves. The second heart sound (S2) marks the beginning of diastole. The third heart sound (S3) and fourth heart sound (S4) are related to filling pressures of the left ventricle during diastole.

Summary

This document discusses, among other things, systems and methods for monitoring heart sounds. One system embodiment includes an implantable heart sound sensor operable to produce an electrical signal representative of at least one heart sound, a heart sound sensor interface circuit coupled to the heart sound sensor to produce a heart sound signal, an implantable posture sensor operable to produce an electrical signal representative of a patient's posture, and a controller circuit. The controller circuit is coupled to the heart sound sensor interface circuit and the posture circuit and is operable to measure the at least one heart sound in correspondence with at least one sensed patient posture.

One method embodiment includes sensing at least one heart sound using an implantable medical device, determining posture information of a patient using the implantable medical device, and measuring the heart sound in correspondence with the posture information.

This summary is intended to provide an overview of the subject matter of the present patent application. It is not intended to provide an exclusive or exhaustive explanation of the invention. The detailed description is included to provide further information about the subject matter of the present patent application.

Brief Description of the Drawings

- FIG. 1 illustrates an embodiment of a system that uses an implantable medical device.
 - FIG. 2 is a graph of heart sound data.
- FIG. 3 shows portions of an embodiment of a system for monitoring heart sounds.

FIG. 4 shows portions of another embodiment of a system for monitoring heart sounds.

FIG. 5 is a block diagram of an embodiment of a method for monitoring heart sounds.

Detailed Description

In the following detailed description, reference is made to the accompanying drawings which form a part hereof, and specific embodiments in which the invention may be practiced are shown by way of illustration. It is to be understood that other embodiments may be used and structural or logical changes may be made without departing from the scope of the present invention.

Monitoring of heart sounds aids caregivers in determining the condition of a patient's heart. For example, chronic changes in S3 amplitude is correlated to left ventricular chamber stiffness and degree of restrictive filling. For a patient with congestive heart failure (CHF), S3 heart sounds become louder as the disease progresses. IMDs can include sensors to assist caregivers in monitoring internal patient parameters such as heart sounds. However, heart sound amplitude varies with patient posture. The present inventors have recognized a need for improved measurement of heart sounds.

The present application discusses, among other things, systems and methods for monitoring heart sounds. FIG. 1 illustrates an embodiment of a system 100 that uses an IMD 110. The system 100 shown is one embodiment of portions of a system 100 used to treat a cardiac arrhythmia or otherwise improve heart function. A pulse generator (PG) or other IMD 110 is coupled by a cardiac lead 108, or additional leads, to a heart 105 of a patient 102. Examples of IMD 110 include, without limitation, a pacer, a defibrillator, a cardiac resynchronization therapy (CRT) device, or a combination of such devices. System 100 also includes an IMD programmer or other external system 170 that provides wireless communication signals 160 to communicate with the IMD 110, such as by using radio frequency (RF) or other telemetry signals.

Cardiac lead 108 includes a proximal end that is coupled to IMD 110 and a distal end, coupled by an electrode or electrodes to one or more portions of a heart 105. The electrodes typically deliver cardioversion defibrillation, pacing, resynchronization therapy, or combinations thereof to at least one chamber of the

heart 105. IMD 110 includes components that are enclosed in a hermetically-sealed canister or "can." Additional electrodes may be located on the can, or on an insulating header, or on other portions of IMD 110, for providing unipolar pacing and/or defibrillation energy in conjunction with the electrodes disposed on or around heart 105. The lead 108 or leads and electrodes are also used for sensing electrical activity of a heart 105.

Implantable heart sound sensors are generally implantable acoustic sensors that convert the detected sounds of the heart into electrical signals. An example of an acoustic sensor is an accelerometer mounted within the can. The amplitude of the several heart sounds as measured by acoustic sensors typically varies significantly with the posture of the patient when the measurement is taken. This typically confounds use of heart sound information.

FIG. 2 is a graph 200 of heart sound data taken from nineteen individuals. The data is a measure of S3 heart sounds using an accelerometer heart sound sensor while the individuals were in four postures: seated (s), recumbent (r), left recumbent (lr), and right recumbent (rr). The individuals were upright when seated, and were at an angle from 0° to 45° when recumbent. Left recumbent refers to the individual being recumbent laterally on their left side and right recumbent refers to an individual being recumbent laterally on their right side. The heart sound sensor was mounted externally on the individuals on the left side of the chest near their pectoral region. The force on the sensor was measured in milli-Gs ("G" refers to G-force, i.e. the average acceleration produced by gravity at the earth's surface). The measurements shown are peak-to-peak amplitudes.

The graph 200 shows that a change in posture for some patients can result in a change as high as 100%-200% in measured S3 amplitudes. These changes in amplitudes due to posture are caused both by changes in coupling of the heart sound sensor to the surrounding tissue and hemodynamic changes in the circulatory system. Hemodynamic changes in the circulatory system cause changes in stiffness of tissue. Because this tissue is the medium for heart sounds to propagate to the sensor, changes in the stiffness of the tissue changes the ability of the heart sound vibrations to travel through the tissue and reach the sensor. If patient posture is not accounted for in heart sound measurements, the

posture dependence may mask changes in heart sounds that are actually due to disease progression, such as the increase in S3 amplitude due to CHF.

FIG. 3 shows portions of an embodiment of a system 300 for monitoring heart sounds. The system 300 includes a device that in turn includes an implantable heart sound sensor 310, a heart sound sensor interface circuit 320 coupled to the heart sound sensor 310, an implantable posture sensor 330, and a controller circuit 340 coupled to the heart sound sensor interface circuit 320 and the implantable posture sensor 330. The implantable heart sound sensor 310 is operable to produce an electrical signal representative of at least one heart sound that is associated with mechanical activity of a patient's heart. In some embodiments, the implantable heart sound sensor 310 includes an accelerometer. In some embodiments, the heart sound sensor 310 includes a strain gauge. In some embodiments, the heart sound sensor 310 includes a microphone. The heart sound sensor interface circuit 320 provides signals representative of one or more heart sounds to the controller circuit 340. Measurements of the signals are made in relation to a physiological event, such as synchronizing the measurement to a sensed heart depolarization. Descriptions of making heart sound measurements in relation to heart depolarization are found in U.S. Patent Application Ser. No. 10/334,694 entitled, "Method and Apparatus for Monitoring of Diastolic Hemodynamics," which is hereby incorporated by reference.

The implantable posture sensor 330 is operable to produce an electrical signal representative of a patient's posture. In some embodiments, the posture sensor 330 includes at least one DC responsive accelerometer. In some embodiments, the posture sensor 330 includes a multi-axis DC responsive accelerometer sensor. In some embodiments, the posture sensor 330 includes a mechanical tilt switch. The controller circuit 340 is operable to measure at least one heart sound in correspondence with at least one sensed patient posture using the heart sound sensor and the posture sensor. The heart sound includes at least one of the S1, S2, S3, and S4 heart sounds. In some embodiments, a heart sound measurement includes a measure of the amplitude of the heart sound signals. In some embodiments, a heart sound measurement includes sampling of the heart sound during a window of time when the heart sound occurs.

The controller circuit 340 is operable to detect a posture of the patient from a signal or signals provided by the posture sensor 330. The controller

circuit 340 is operable by executing an algorithm or algorithms implemented by hardware, software, firmware or any combination of hardware, software or firmware. In some embodiments, the controller 340 executes a heart sound measurement in relation to a time of day, such as when a patient is likely to be asleep for example. In some embodiments, the measurement is made occasionally or periodically throughout the day, such as hourly. In some embodiments, the measurement is made in relation to a change in posture.

According to some embodiments, the controller is operable to measure the at least one heart sound while the patient is in an upright posture. In some embodiments, the controller 340 only executes a heart sound measurement when an upright posture is detected in the patient. An upright posture refers to a standing or a seated posture for example. In some embodiments, the device further includes a memory circuit coupled to the controller 340, and the controller 340 only stores a heart sound measurement when an upright posture is detected.

In some embodiments, the controller is operable to measure a heart sound in a plurality of postures. The heart sound measurement is made in correspondence with patient posture. In some embodiments, the heart sound measurement is stored in correspondence with a patient posture. For example, the controller 340 stores a set of heart sound measurements made when the patient is in a supine position and stores a set of heart sound measurements made when the patient is in an upright position. In another example, the controller 340 stores heart sound measurements made when the patient is in a recumbent position and when a patient is in an upright position. In some embodiments, heart sound measurements are categorized, or "binned," according to posture. Trends in the heart sounds are then determined by comparing measurements in the same "bin." Thus, problems associated with interpreting a set of heart sound measurements from varying postures are avoided.

In some embodiments, a scaling factor is applied to a heart sound measurement. The scaling factor is determined as a function of posture. The scaling factor is applied to the heart sound measurements to remove the variation with posture. For example, if S2 heart sounds for a patient in an upright position are found to have one-half the amplitude of S2 heart sounds for the patient in a recumbent position, the upright heart sound measurements are multiplied by a

scaling factor of two while the recumbent heart sound measurements are multiplied by a scaling factor of one or left unaltered. If the variation with posture is removed through scaling, trends in the heart sounds can then be determined by comparing measurements directly without regard to a particular posture or bin.

According to some embodiments, the heart sounds may be stored according to seated, recumbent, and supine postures, and further, according to left and right lateral orientations. In some embodiments, the number of postures detected by the system 300 may be limited by the performance of the implantable posture sensor 330. For example, the posture sensor 330 may only be able to detect the difference between an upright posture and a supine posture. In another example, the posture sensor 330 may only be able to detect one of several postures with an accuracy of 15°. In such a case, the controller circuit 340 could be programmed to define supine as 0° to 30° as measured from the horizontal, recumbent as 30° to 60° and upright as 60° to 90°. In another example, the posture sensor 330 may be unable to detect a lateral orientation of a patient. Use of posture sensors may involve calibrating the sensors to the patient. A caregiver may put a patient in the different postures to calibrate the response of the sensor to detect that posture.

Heart sound measurements are susceptible to noise from movement and other non-cardiac vibrations such as talking. According to some embodiments, the heart sound sensor 310 is used to detect mechanical interference from non-cardiac vibrations. The controller circuit 340 uses signals provided by the heart sound sensor 310 to determine that the interference level is below a threshold interference level before a heart sound measurement is executed. In some embodiments, the controller circuit 340 determines the level of interference by monitoring the heart sound signal outside of a window of time when the heart sound occurs. In some embodiments, the controller circuit 340 determines the level of interference by a method that includes averaging the heart sound signal over a period of time. In some embodiments, the controller circuit 340 determines the level of interference by a method that includes digital signal processing (DSP) of the heart sound signal, such as to extract spectral components associated with heart sounds from interfering sounds.

Heart sound measurements are less susceptible to noise and interference from artifacts of patient movement if they are taken during a period of patient inactivity. To determine patient inactivity, some embodiments of the device further include an implantable activity sensor, such as an accelerometer (which can be the same accelerometer as the heart sound sensor or a different accelerometer). The activity sensor detects a level of patient physical activity. The controller circuit 340 is operable to measure at least one heart sound in correspondence with at least one sensed patient posture when a patient activity level is below a specified activity threshold value. For example, if the controller circuit 340 is operable to take a heart sound measurement every fifteen minutes, the controller circuit 340 may first determine if the patient is in an upright position and is inactive before executing the measurement. In some embodiments, the activity sensor is different from the heart sound sensor 310. In other embodiments, the activity sensor is the same as the heart sound sensor 310 and patient activity is determined by signal processing to isolate the activity signals.

Patient inactivity can also be determined or inferred by the time of day. Thus, in some embodiments, the device further includes a clock circuit and the controller circuit 340 is operable to measure heart sounds when it is likely that a patient is sleeping.

Patient inactivity can also be determined from other physiologic parameters. For example, a low patient heart rate may be an indication of patient inactivity. Thus, in some embodiments, the device further includes at least one implantable cardiac signal sensing circuit. The cardiac signal sensing circuit is operable to detect at least one intrinsic cardiac signal, and the controller circuit 340 is operable to measure the at least one heart sound in correspondence with at least one sensed patient posture when a patient heart rate is below a specified heart rate threshold value.

In some embodiments, patient inactivity is determined from the heart sound themselves. The controller circuit 340 detects heart sounds but waits to measure and store a heart sound until the heart sounds indicates the patient is inactive. In some embodiments, the controller makes and stores a heart sound measurement when a period of time between heart sounds are longer than a

threshold period, i.e. when a heart, as determined by heart sounds, is below a threshold rate.

Patient inactivity can also be determined from a patient breathing rate. Thus, in some embodiments, the implantable medical device further includes a trans-thoracic impedance measurement circuit to provide a trans-thoracic impedance signal of a subject. The controller circuit 340 is operable to determine breathing volume from the trans-thoracic impedance signal, and to measure the at least one heart sound in correspondence with at least one sensed patient posture when a patient breathing rate is below a specified breathing rate threshold value. Illustrative examples of methods of monitoring lung tidal volume by measuring trans-thoracic impedance are described in Hartley et al. U.S. Patent No. 6,076,015 entitled "RATE ADAPTIVE CARDIAC RHYTHM MANAGEMENT DEVICE USING TRANSTHORACIC IMPEDANCE," which is incorporated herein by reference.

According to some embodiments, one or more heart sound measurements are combined with one or more measurements of one or more other physiologic sensors, such as a trans-thoracic impedance sensor or a cardiac signal sensor, to provide a measurement of patient health. In some embodiments, one or more heart sound measurements are combined with one or more measurements of other physiologic sensors in correspondence with at least one sensed patient posture. As an example of such embodiments, trending of heart sound measurements can be combined with trans-thoracic impedance measurements in correspondence with at least one sensed patient posture to track the condition of a congestive heart failure patient. As another example, the trans-thoracic impedance measurement circuit provides a measurement of near-DC transthoracic impedance, and the controller is operable to provide the near-DC transthoracic impedance measurement in correspondence with at least one sensed patient posture and the heart sound measurement. Illustrative examples of methods of monitoring near-DC trans-thoracic impedance are described in Stahmann et al. U.S. Patent Application Ser. No. 10/921,503 entitled "THORACIC IMPEDANCE DETECTION WITH BLOOD RESISTIVITY COMPENSATION," which is incorporated herein by reference. Other examples of measurements of other physiologic sensors include using a measure of hematocrit in blood of the subject, or using a measure of resistivity of blood

within a heart.

FIG. 4 shows portions of an embodiment of a system 400 for monitoring heart sounds. The system 400 includes an implantable device 405 and an external device 410 operable to communicate with the implantable device 405. The implantable device 405 includes a heart sound sensor 415, a heart sound sensor interface circuit 420, and posture sensor 425 coupled to control circuit 430. The controller circuit 430 is operable to measure the at least one heart sound in correspondence with at least one sensed patient posture. The implantable device 405 also includes a memory circuit 435, a sensing circuit 440, and a therapy circuit 445. The memory circuit 435 stores heart sound measurements. The sensing circuit 440 is coupled to a cardiac lead or leads to sense cardiac signals from a subject's heart. The therapy circuit 445 is attached to a cardiac lead or leads to provide cardioversion defibrillation, pacing, resynchronization therapy, or combinations thereof to at least one chamber of the heart.

In an embodiment, the controller circuit 430 measures the S3 heart sounds using the heart sound sensor 415 for the purpose of monitoring ventricular diastolic hemodynamic performance over time. By monitoring the posture sensor 425, the controller circuit 430 measures the S3 heart sounds while the patient is in an upright posture to reduce variations in the measurements due to patient posture. Based on the S3 heart sound measurements, the controller circuit 430 controls delivery of at least one therapy, such as pacing resynchronization therapy for example, using the therapy circuit 445.

The implantable device 405 further includes a communication circuit 450. The external device 410 communicates wirelessly with the implantable device 405 by using radio frequency (RF) or other telemetry signals. The implantable device 405 communicates heart sound information to the external device 410. In some embodiments, the external device 410 is part of, or is in communication with, a computer network such as a hospital computer network or the internet. According to some embodiments, the external device 410 is operable to communicate an alarm based on the heart sound information and the posture information. In some embodiments, the alarm includes an audio alarm or a visual alarm indication. In some embodiments, an alarm is communicated via the network to a caregiver.

According to some embodiments, the external device 410 includes a display operable to display heart sound information in relation to sensed patient posture. In some embodiments, the heart sound information includes a trend of heart sound information in relation to patient posture. The trend information is useful to establish a trend indicative of a disease status of a patient or subject. This status can be an indication of worsening status or improving status.

In some embodiments, the trend information consists entirely of heart sound information corresponding to a single posture. In some embodiments, the trend information consists of heart sound information corresponding to a range of postures, e.g., the range from a recumbent posture to an upright posture. In some embodiments, a trend is maintained for each posture. In some embodiments, heart sound variation with posture is removed by using one or more scaling factors and the heart sound information is combined into a single trend. In some embodiments, the trend or trends of heart sound information is maintained in the implantable device 405, the external device 410, or both. In some embodiments, analyses on the heart sound information for multiple separate trends, such as a separate trend for each of supine, seated, and recumbent postures are combined to form a single decision as to whether to generate an alarm. In some embodiments, the analyses are combined with one or more measurements of one or more other physiologic sensors. These analyses can be done in the implantable device 405, the external device 410, or both.

FIG. 5 is a block diagram of an embodiment of a method 500 for monitoring heart sounds. At 510, at least one heart sound is sensed using an implantable medical device. In some embodiments, sensing at least one heart sound includes sensing at least one of the S1, S2, S3, and S4 heart sounds, and the measurement of at least one heart sound is performed when a heart rate is below a specified heart rate threshold value. In some embodiments, the measurement of at least one heart sound is performed when a patient activity level is below a specified activity threshold value. In some embodiments, the measurement of at least one heart sound is performed when a mechanical interference level is below a threshold value.

At 520, posture information of a patient is determined using the implantable medical device, and at 530, the heart sound is measured in correspondence with the posture information. In some embodiments, measuring

at least one heart sound in correspondence with the posture information includes measuring heart sounds in correspondence with respective postures and relating a heart sound measurement to a particular posture. In some embodiments, measuring the at least one heart sound in correspondence with respective postures includes applying at least one scaling factor as a function of posture to at least one heart sound measurement. In some embodiments, measuring at least one heart sound in correspondence with the patient's posture includes measuring the heart sound contingent on the patient being in a specified posture, such as for example an upright posture.

According to some embodiments, measuring at least one heart sound in correspondence with the patient's posture includes measuring at least one trend of heart sounds in relation to posture. In some embodiments the heart sound trend information is combined with trending of measurements from other physiologic sensors. In some embodiments, trending information of measurements of the at least one heart sound is stored in correspondence with the patient's posture. In some embodiments, the method 500 further includes communicating the trending information to an external device for display.

The accompanying drawings that form a part hereof, show by way of illustration, and not of limitation, specific embodiments in which the subject matter may be practiced. The embodiments illustrated are described in sufficient detail to enable those skilled in the art to practice the teachings disclosed herein. Other embodiments may be utilized and derived therefrom, such that structural and logical substitutions and changes may be made without departing from the scope of this disclosure. This Detailed Description, therefore, is not to be taken in a limiting sense, and the scope of various embodiments is defined only by the appended claims, along with the full range of equivalents to which such claims are entitled.

Such embodiments of the inventive subject matter may be referred to herein, individually and/or collectively, by the term "invention" merely for convenience and without intending to voluntarily limit the scope of this application to any single invention or inventive concept if more than one is in fact disclosed. Thus, although specific embodiments have been illustrated and described herein, it should be appreciated that any arrangement calculated to achieve the same purpose may be substituted for the specific embodiments

shown. This disclosure is intended to cover any and all adaptations, or variations, or combinations of various embodiments. Combinations of the above embodiments, and other embodiments not specifically described herein, will be apparent to those of skill in the art upon reviewing the above description.

The Abstract of the Disclosure is provided to comply with 37 C.F.R. §1.72(b), requiring an abstract that will allow the reader to quickly ascertain the nature of the technical disclosure. It is submitted with the understanding that it will not be used to interpret or limit the scope or meaning of the claims. In addition, in the foregoing Detailed Description, it can be seen that various features are grouped together in a single embodiment for the purpose of streamlining the disclosure. This method of disclosure is not to be interpreted as reflecting an intention that the claimed embodiments require more features than are expressly recited in each claim. Rather, as the following claims reflect, inventive subject matter lies in less than all features of a single disclosed embodiment. Thus the following claims are hereby incorporated into the Detailed Description, with each claim standing on its own.

What is claimed is:

1. A system comprising:

a device comprising:

an implantable heart sound sensor operable to produce an electrical signal representative of at least one heart sound, the heart sound associated with mechanical activity of a patient's heart;

a heart sound sensor interface circuit coupled to the heart sound sensor to produce a heart sound signal;

an implantable posture sensor operable to produce an electrical signal representative of a patient's posture; and

a controller circuit, coupled to the heart sound sensor interface circuit and the posture circuit, wherein the controller circuit is operable to measure the at least one heart sound in correspondence with at least one sensed patient posture.

- 2. The system of claim 1, wherein the controller is operable to measure the heart sound in an upright posture.
- 3. The system of claim 1, wherein the controller is operable to measure the heart sound in a plurality of postures.
- 4. The system of claim 3, wherein the device further includes a storage circuit coupled to the controller, and wherein the controller is operable to store at least one heart sound measurement in correspondence with patient posture.
- 5. The system of claim 3, wherein the controller is operable to apply a scaling factor to at least one heart sound measurement, wherein the scaling factor is a function of a patient posture.
- 6. The system of claim 1, wherein the device further includes a clock circuit and the controller circuit is operable to measure heart sounds at a time of day when a patient is in a recumbent posture.

7. The system of claim 1, wherein the controller circuit is operable to use the electrical signal provided by the implantable heart sound sensor to determine that the interference is below a threshold level before a heart sound measurement is executed.

- 8. The system of claim 1, wherein the device further includes at least one implantable cardiac signal sensing circuit operable to detect at least one intrinsic cardiac signal, and wherein the controller is operable to measure the at least one heart sound in correspondence with at least one sensed patient posture when a patient heart rate is below a specified heart rate threshold value.
- 9. The system of claim 1, wherein the device further includes an implantable activity sensor and the controller is operable to measure the at least one heart sound in correspondence with at least one sensed patient posture when a patient activity level is below a specified activity threshold value.
- 10. The system of claim 1, wherein the device further includes an implantable trans-thoracic impedance measurement circuit to provide a transthoracic impedance signal of a subject, wherein the controller is operable to provide the trans-thoracic impedance measurement in correspondence with at least one sensed patient posture and the measured heart sound.
- 11. The system of claim 10, wherein the trans-thoracic impedance measurement circuit provides a measurement of near-DC trans-thoracic impedance and the controller is operable to provide the near-DC trans-thoracic impedance measurement in correspondence with at least one sensed patient posture and the measured heart sound.
- 12. The system of claim 1, wherein the device is an implantable device that includes a communication circuit to communicate with an external device, and wherein the system further includes the external device, and wherein the external device includes a display to display heart sound information in relation to sensed patient posture.

13. The system of claim 12, wherein the heart sound information includes at least one trend of heart sound information in relation to patient posture.

- 14. The system of claim 1, wherein the device is an implantable device that includes a communication circuit to communicate with an external device, and wherein the system further includes the external device, and wherein the external device is in communication with a computer network.
- 15. The system of claim 14, wherein the external device is operable to communicate an alarm based on information that includes the heart sound signal and the patient posture.
- 16. The system of claim 1, wherein the controller circuit includes a categorization module to categorize the heart sound according to posture.
- 17. The system of claim 1, wherein the controller circuit initiates a heart sound measurement contingent on a specified patient posture.
- 18. The system of claim 17, wherein the specified patient posture includes an upright patient posture.
- 19. A method comprising:

sensing at least one heart sound using an implantable medical device; determining posture information of a patient using the implantable medical device; and

measuring the heart sound in correspondence with the posture information.

20. The method of claim 19, wherein measuring the at least one heart sound in correspondence with the posture information includes measuring heart sounds in correspondence with respective postures and relating a heart sound measurement to a posture.

21. The method of claim 20, wherein measuring the at least one heart sound in correspondence with respective postures includes applying at least one scaling factor to at least one heart sound measurement, wherein the scaling factor is a function of posture.

- 22. The method of claim 19, comprising excluding at least one heart sound measurement when a corresponding heart rate is above a specified heart rate threshold value.
- 23. The method of claim 19, wherein measuring at least one heart sound in correspondence with the patient's posture includes measuring the heart sound contingent on the patient being in a specified posture.
- 24. The method of claim 23, wherein the specified posture is an upright posture.
- 25. The method of claim 19, comprising excluding at least one heart sound measurement when a patient activity level is above a specified activity threshold value.
- 26. The method of claim 19, comprising excluding at least one heart sound measurement when a mechanical interference level exceeds a threshold value.
- 27. The method of claim 19, wherein the measuring at least one heart sound in correspondence with the patient's posture includes measuring a trend of heart sounds in relation to posture.
- 28. The method of claim 19, further including storing trending information of measurements of the at least one heart sound in correspondence with the patient's posture.
- 29. The method of claim 28, further including communicating the trending information to an external device for display.

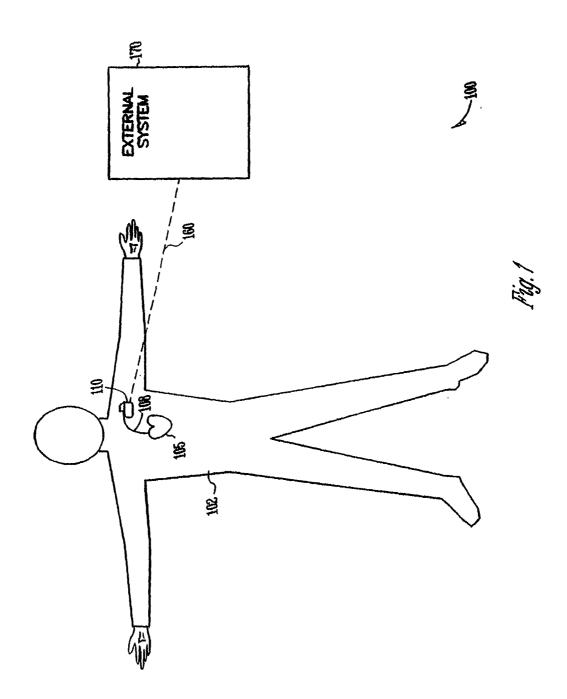
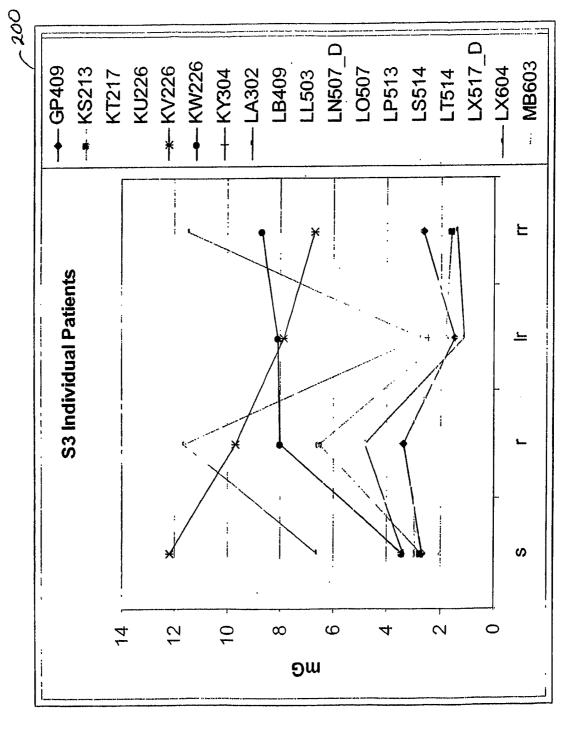
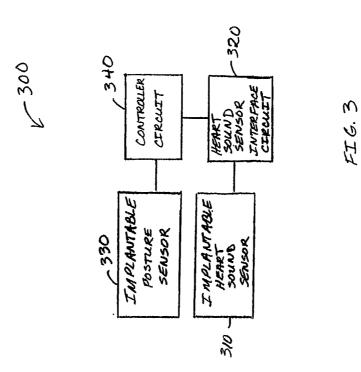
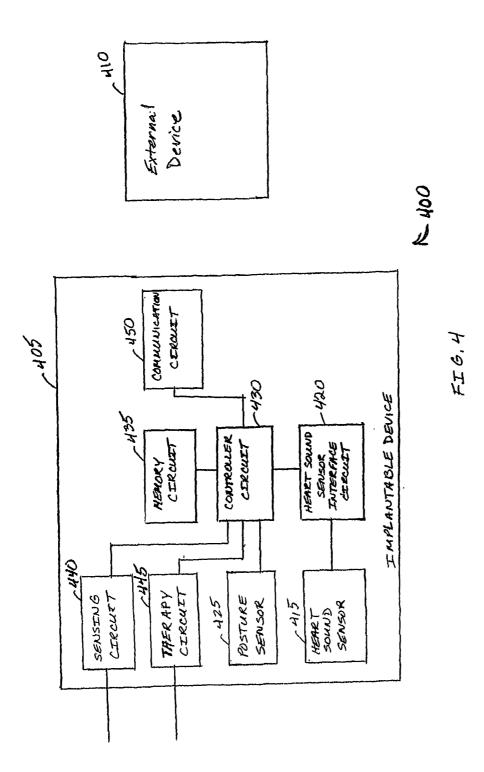
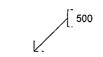


FIG. 2









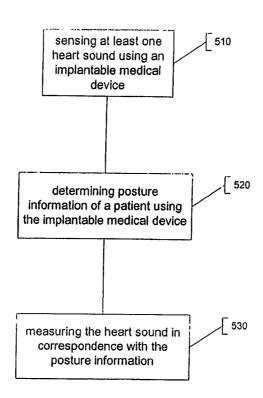


FIG. 5

INTERNATIONAL SEARCH REPORT

International application No PCT/US2006/001801

A. CLASSIFICATION OF SUBJECT MATTER INV. A61B7/04 According to International Patent Classification (IPC) or to both national classification and IPC **B. FIELDS SEARCHED** Minimum documentation searched (classification system followed by classification symbols) A61N A61B Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched Electronic data base consulted during the International search (name of data base and, where practical, search terms used) EPO-Internal, PAJ C. DOCUMENTS CONSIDERED TO BE RELEVANT Category* Citation of document, with indication, where appropriate, of the relevant passages Relevant to claim No. X US 5 554 177 A (KIEVAL ET AL) 1-3,6,7,10 September 1996 (1996-09-10) 19,20 column 5, line 18 - line 44 column 6, line 41 - line 60; figure 5 Υ 4.6 - 15.17,18, 22-29 Α 5,16,21 Υ US 2004/127792 A1 (SIEJKO KRZYSZTOF Z ET 4,6-15, AL) 1 July 2004 (2004-07-01) 17,18, cited in the application 22 - 29paragraphs [0030], [0041], [0042], [0045] X Further documents are listed in the continuation of Box C. See patent family annex. Special categories of cited documents: "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the "A" document defining the general state of the art which is not considered to be of particular relevance invention "E" earlier document but published on or after the international "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "Y" document of particular relevance; the claimed invention cannets of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. document referring to an oral disclosure, use, exhibition or other means document published prior to the international filing date but later than the priority date claimed "&" document member of the same patent family Date of the actual completion of the international search Date of mailing of the international search report 7 June 2006 16/06/2006 Name and mailing address of the ISA/ Authorized officer European Patent Office, P.B. 5818 Patentlaan 2 NL – 2280 HV Rijswijk Tel. (+31–70) 340–2040, Tx. 31 651 epo nl, Fax: (+31–70) 340–3016 Petter, E

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International application No PCT/US2006/001801

C(Continua	inuation). DOCUMENTS CONSIDERED TO BE RELEVANT			
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