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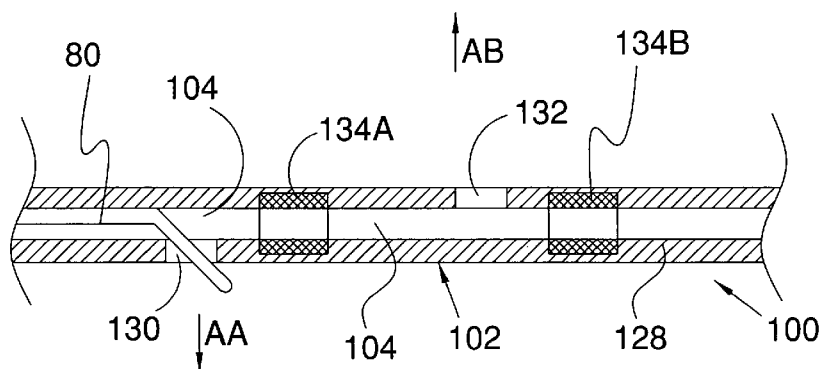


FIG. 14

(57) Abstract: The present disclosure is directed to an apparatus. The apparatus may include a first intravascular device (100) having a distal portion. The distal portion including at least one aperture (230), at least one radiopaque marker (132, 134), and at least one orienting element (220). The apparatus may further include a reentry device (80) having a body and a distal tip.

**ENDOVASCULAR DEVICES AND METHODS FOR EXPLOITING
INTRAMURAL SPACE**

DESCRIPTION OF THE INVENTION

CROSS-REFERENCE TO RELATED APPLICATION

This PCT application claims the benefit of U.S. Patent Application No. 12/222,737 filed August 14, 2008, which is herein incorporated by reference in its entirety. That application, in turn, is a continuation-in-part of, and claims the benefit under 35 U.S.C. §§ 120, 365(c) of, PCT International Application No. PCT/US2007/024209, filed November 20, 2007, which is herein incorporated by reference in its entirety and which claims the benefit of U.S. Provisional Application No. 60/964,765, filed August 14, 2007, U.S. Provisional Application No. 60/905,849, filed March 9, 2007, and U.S. Provisional Application No. 60/860,416, filed November 21, 2006, all of which are herein incorporated by reference in their entirety.

FIELD OF THE INVENTION

The inventions described herein relate to devices and associated methods for the treatment of chronic total occlusions. More particularly, the inventions described herein relate to devices and methods for crossing chronic total occlusions and establishing a pathway blood flow past the chronic total occlusions.

BACKGROUND OF THE INVENTION

Due to age, high cholesterol and other contributing factors, a large percentage of the population has arterial atherosclerosis that totally occludes portions of the patient's vasculature and presents significant risks to patient health. For example, in the case of a total occlusion of a coronary artery, the result may be painful angina, loss of cardiac tissue or patient death. In another example, complete occlusion of the femoral and/or popliteal arteries in the leg may result in limb threatening ischemia and limb amputation.

Commonly known endovascular devices and techniques are either inefficient (time consuming procedure), have a high risk of perforating a vessel (poor safety) or fail to cross the occlusion (poor efficacy). Physicians currently have difficulty visualizing the native vessel lumen, can not accurately direct endovascular devices toward the visualized lumen, or fail to advance devices through the lesion. Bypass surgery is often the preferred treatment for patients with chronic total occlusions, but less invasive techniques would be preferred.

BRIEF DESCRIPTION OF THE FIGURES

Figure 1 is a somewhat stylized representation of a human heart. The heart includes a plurality of coronary arteries, all of which are susceptible to occlusion.

Figure 2 is an enlarged view further illustrating a portion of the heart shown in the previous figure. In figure 2, a total occlusion is shown within a coronary artery.

Figure 3 is a perspective view of a blood vessel (e.g., a coronary artery). In figure 3, the wall of the blood vessel is shown having three layers (the intima, the media, and the adventitia).

Figure 4 is a lateral cross-sectional view of the artery shown in the previous figure. In figure 4, an orienting device is shown disposed between the adventitia and the intima of the artery.

Figure 5 is a longitudinal cross-sectional view of an artery having an occlusion blocking the true lumen.

Figure 6 is an additional cross-sectional view of the artery shown in the previous figure. In the embodiment of figure 6, a crossing device has been advanced over a guidewire so that a distal portion of crossing device is disposed in proximal segment of the true lumen.

Figure 7 is a plan view showing an assembly including crossing device shown in the previous figure.

Figure 8 is an additional view of an artery. In the embodiment of figure 8, the distal end of the crossing device has been advanced in a distal direction so that the tip of the crossing device is adjacent an occlusion that is blocking the true lumen of the artery.

Figure 9 is an additional view of the artery and the crossing device shown in the previous figure. In the embodiment of figure 9, the distal end of the crossing device has been advanced between the intima and the adventitia of the wall of the artery.

Figure 10 is an additional view of the artery shown in the previous figure. In the embodiment of figure 10, the crossing device has been withdrawn and a guidewire remains in the position formerly occupied by the crossing device.

Figure 11 is an additional view of the artery and the guidewire shown in the previous figure. In the embodiment of figure 11, an orienting device 100 been advanced over the guidewire.

Figure 12 is an additional view of the artery and the orienting device shown in the previous figure.

Figure 13 is an additional view showing the orienting device shown in the previous figure. In the embodiment of figure 13 a re-entry device has been advanced into a central lumen of the orienting device. A distal end of the re-entry device has been advanced through a first aperture of the orienting device and can be seen residing in the true lumen.

Figure 14 is an enlarged cross-sectional view of the orienting device shown in the previous figure.

Figure 15 is a stylized plan view showing the orienting device shown in the previous figure.

Figure 16 is a perspective view of an additional exemplary embodiment of an orienting device.

Figure 17 is a plan view showing an additional exemplary orienting device.

Figure 18 is a stylized perspective view showing a portion of the orienting device shown in the previous figure. For purposes of illustration, the portion shown in figure 18 is created by cutting the orienting device along cutting plane A-A and cutting plane B-B shown in the previous figure.

Figure 19 is a stylized cross-sectional view showing the orienting device shown in the previous figure. In the embodiment of figure 20, an orienting element of the orienting device is assuming a deployed shape.

Figure 20 is an additional stylized cross-sectional view showing the orienting device shown in the previous figure. In the embodiment of figure 20, an orienting element of the orienting device is assuming a generally collapsed shape.

Figure 21 is a plan view showing an additional exemplary orienting device.

BRIEF SUMMARY

Described herein are devices and methods employed to exploit the vascular wall of a vascular lumen for the purpose of bypassing a total occlusion of an artery. Exploitation of a vascular wall may involve the passage of an endovascular device into and out of said wall which is commonly and interchangeable described as false lumen access, intramural access, submedial access or in the case of this disclosure, subintimal access.

In one aspect, the present disclosure is directed to a device. The device may include a distal shaft defining a central lumen and an orienting element comprising at least one inflatable member. Wherein a first portion of the orienting element extending from the shaft in a first direction and a second portion of the orienting element extending from the

shaft in a second direction. Further, wherein the second direction is substantially opposite the first direction.

In another aspect, the present disclosure is directed to a device. The device may include a distal shaft defining a central lumen and an orienting element comprising a first inflatable member and a second inflatable member. Wherein the first inflatable member extending from the shaft in a first direction and the second inflatable member extending from the shaft in a second direction. Further, wherein the second direction is substantially opposite the first direction.

In yet another aspect, the present disclosure is directed to a method. The method may include providing a device comprising a distal shaft and an orienting element, and positioning the orienting element of the device between an occlusion and an adventitia of a blood vessel. The method may further include inflating an inflatable member of the orienting element to orient the device relative to a true lumen of the blood vessel, and advancing a re-entry device through a lumen defined by the device. The method may still further include advancing a distal end of a re-entry device through an aperture of the device, and wherein the aperture is substantially orthogonal to a plane defined by the orienting element.

DETAILED DESCRIPTION OF EXEMPLARY EMBODIMENTS

The following detailed description should be read with reference to the drawings in which similar elements in different drawings are numbered the same. The drawings, which are not necessarily to scale, depict illustrative embodiments and are not intended to limit the scope of the invention.

Figure 1 is a somewhat stylized representation of a human heart 50. Heart 50 includes a plurality of coronary arteries 52, all of which are susceptible to occlusion. Under certain physiological circumstances and given sufficient time, some occlusions may become total or complete, such as total occlusion 36. As used herein, the terms total occlusion and complete occlusion are intended to refer to the same or similar degree of occlusion with some possible variation in the age of the occlusion. Generally, a total occlusion refers to a vascular lumen that is ninety percent or more functionally occluded in cross-sectional area, rendering it with little to no blood flow therethrough and making it difficult or impossible to pass a conventional guide wire therethrough. Also generally, the older the total occlusion the more organized the occlusive material will be and the more fibrous and calcified it will

become. According to one accepted clinical definition, a total occlusion is considered chronic if it is greater than two weeks old from symptom onset.

Figure 2 is an enlarged view further illustrating a portion of heart 50 shown in the previous figure. In figure 2, a total occlusion 36 is shown within a coronary artery 52. Generally, the proximal segment 32 of artery 52 (i.e., the portion of artery 52 proximal of total occlusion 36) may be easily accessed using endovascular devices and has adequate blood flow to supply the surrounding cardiac muscle. The distal segment 34 of artery 52 (i.e., the portion of artery 52 distal of total occlusion 36) is not easily accessed with interventional devices and has significantly reduced blood flow as compared to proximal segment 32.

Figure 3 is a perspective view of an artery 20 having a wall 22. In figure 3, wall 22 of artery 20 is shown having three layers. The outermost layer of wall 22 is the adventitia 24 and the innermost layer of wall 22 is the intima 26. Intima 26 defines a true lumen 30 of artery 20. The tissues extending between intima 26 and adventitia 24 may be collectively referred to as the media 28. For purposes of illustration, intima 26, media 28 and adventitia 24 are each shown as a single homogenous layer in figure 3. In the human body, however, the intima and the media each comprise a number of sub-layers. The transition between the external most portion of the intima and the internal most portion of the media is sometimes referred to as the subintimal space 40.

With reference to figure 3, it will be appreciated that the subintimal space 40 has a generally annular shape with its radial center at the center of the true lumen. Some of the devices and methods discussed in this detailed description may take advantage of the position and geometry of the subintimal space 40 relative to the true lumen of the blood vessel. For example, some orienting devices described herein may be adapted to orient themselves within that space. Once the orientation of the orienting device is established, the orienting device may be used to direct a re-entry device toward the true lumen.

Figure 4 is a lateral cross-sectional view of artery 20 shown in the previous figure. In figure 4, an orienting device 100 is shown disposed between adventitia 24 and intima 26 of artery 20. Orienting device 100 comprises a distal shaft 102 having an outer wall 128 defining a central lumen 104. Orienting device 100 comprises an orienting element 120 that is coupled to distal shaft 102.

In the embodiment of figure 4, orienting element 120 comprises an inflatable member 126. The top of inflatable member 126 may be fixed to distal shaft 102, for

example, at a first interface 190A. The bottom of inflatable member 126 may be fixed to distal shaft 102, for example, at a second interface 190B.

Orienting element 120 comprises a first portion 106 and a second portion 108. First portion 106 of orienting element 120 extends in a first direction away from distal shaft 102. Second portion 108 of orienting element 120 extends away from distal shaft 102 in a second direction that is generally opposite the first direction.

Distal shaft 102 defines a first aperture 130 and a second aperture 132. First aperture 130 extends in a third direction through distal shaft 102. A second aperture 132 extends through distal shaft 102 in a fourth direction that is generally opposite the third direction. The first aperture 130 and second aperture 132 are generally oriented at a right angle to a tangent plane TP. In figure 4, tangent plane TP is tangent to subintimal space 40.

When inflatable member 126 of orienting element 120 is inflated between adventitia 24 and intima 26 of artery 20 orienting device 100 will orient itself within artery 20 so that either first aperture 130 or second aperture 132 opens toward a true lumen of the artery. In the embodiment of figure 4, orienting device 100 has been positioned so that first aperture 130 opens toward intima 26 of artery 20 and second aperture 132 opens toward adventitia 24. In figure 4, a re-entry device 80 is shown extending through first aperture 130 and intima 26. A distal end of re-entry device 80 is disposed in true lumen 30 of blood vessel 20.

When inflatable member 126 is inflated, the number of directions that first aperture 130 and second aperture 132 may be facing is reduced. This may be conceptualized in terms of degrees of freedom. When inflatable member 126 of orienting element 120 is inflated, the number of directions that an aperture may be facing is reduced from 360 degrees of freedom to two degrees of freedom, 180 degrees apart. Orienting device 100 and re-entry device 80 may be used to establish fluid communication between the proximal segment and the distal segment that are separated by an occlusion. Exemplary methods may be described with reference to figures 5 through 13.

Figure 5 is a longitudinal cross-sectional view of an artery 20 having an occlusion 36 blocking true lumen 30 thereof. Occlusion 36 divides true lumen 30 into a proximal segment 32 and a distal segment 34. In figure 5, a distal portion of a guidewire 60 is shown extending into proximal segment 32 of true lumen 30. The methods described in this document may include the step of advancing a guidewire to a location proximate an occlusion in a blood vessel. The exemplary methods described in this document may also include the step of advancing guidewire 60 between occlusion 36 and adventitia 24 of wall

22. In some cases, however, the nature of the occlusion and the blood vessel will be such that the guidewire is unlikely to advance beyond the occlusion. When this is the case, the guidewire may be used to guide additional endovascular devices to a location proximate occlusion 36.

Figure 6 is an additional cross-sectional view of artery 20 shown in the previous figure. In the embodiment of figure 6, a crossing device 70 has been advanced over guidewire 60 so that a distal portion of crossing device 70 is disposed in proximal segment 32 of true lumen 30. Crossing device 70 of figure 6 comprises a tip 74 that is fixed to a distal end of a shaft 72. Crossing device 70 may be used in conjunction with a method for establishing a channel between proximal segment 32 and distal segment 34. The methods described in this document may include the step of advancing a crossing device over a guidewire.

In some useful methods in accordance with the present disclosure, crossing device 70 may be rotated about its longitudinal axis and moved in a direction parallel to its longitudinal axis simultaneously. When this is the case, rotation of crossing device 70 may reduce resistance to the axial advancement of crossing device 70. These methods take advantage of the fact that the kinetic coefficient of friction is usually less than the static coefficient of friction for a given frictional interface. Rotating crossing device 70 assures that the coefficient of friction at the interface between the crossing device and the surrounding tissue will be a kinetic coefficient of friction and not a static coefficient of friction.

Figure 7 is a plan view showing an assembly including crossing device 70 shown in the previous figure. In the embodiment of figure 7, a handle assembly 150 is coupled to crossing device 70. In figure 7, handle assembly 150 is shown disposed about a proximal portion of a shaft 152 of crossing device 70. In figure 7, a portion of handle assembly 150 is positioned between the thumb and forefinger of a left hand LH. A second portion of handle assembly 150 is disposed between the thumb and forefinger of a right hand RH. With reference to figure 7, it will be appreciated that handle assembly 150 is long enough to receive the thumb and forefingers of a physician's right and left hands. When this is the case, a physician can use two hands to rotate handle assembly 150.

Rotation of crossing device 70 can be achieved by rolling handle assembly 150 between the thumb and forefinger of one hand. Two hands may also be used to rotate handle assembly 150 as shown in figure 7. In some useful methods, crossing device 70 can be rotated and axially advanced simultaneously.

In some useful methods in accordance with the present disclosure, crossing device 70 is rotated at a rotational speed of between about 2 revolutions per minute and about 200 revolutions per minute. In some particularly useful methods in accordance with the present disclosure, crossing device 70 is rotated at a rotational speed of between about 50 revolutions per minute and about 150 revolutions per minute.

Crossing device 70 may be rotated by hand as depicted in figure 7. It is also contemplated that a mechanical device (e.g., an electric motor) may be used to rotate crossing device 70. Rotating crossing device 70 assures that the coefficient of friction at the interface between the crossing device and the surround tissue will be a kinetic coefficient of friction and not a static coefficient of friction.

Figure 8 is an additional longitudinal cross-sectional view of an artery 20. In the embodiment of figure 8, the distal end of crossing device 70 has been advanced in a distal direction so that tip 74 is adjacent occlusion 36. With reference to figure 8, it will be appreciated that tip 74 has passed beyond intima 26 and is disposed between occlusion 36 and adventitia 24 of artery 20. Some methods described in this document may include the step of advancing a crossing device between an occlusion and the adventitia of an artery.

Figure 9 is an additional view of artery 20 and crossing device 70 shown in the previous figure. In the embodiment of figure 9, the distal end of crossing device 70 has been advanced in an axial direction past occlusion 36. Methods described herein may include the step of advancing a crossing device beyond an occlusion. In the embodiment of figure 9, crossing device has crossed occlusion 36 by advancing between occlusion 36 and adventitia 24 of wall 22.

It is to be appreciated that other methods of crossing an occlusion are within the spirit and scope of this disclosure. For example, the crossing device 70 may pass through occlusion 36 while remaining disposed inside true lumen 30. In figure 9, tip 74 of crossing device 70 is shown residing between intima 26 and adventitia 24 of artery 20. As tip 74 moves in an axial direction between intima 26 and adventitia 24, tip 74 may cause blunt dissection of the layers forming wall 22 of artery 20. Alternatively, tip 74 may cause blunt dissection of the materials comprising the occlusion 36.

In the embodiment of figure 9, tip 74 of crossing device 70 is disposed between intima 26 and adventitia 24. When this is the case, fluid communication between proximal segment 32 and distal segment 34 may be achieved by creating an opening through intima 26. Such an opening may be created, for example, using a re-entry device and an orienting device that directs the advancement of the re-entry device toward intima 26.

Figure 10 is an additional view of artery 20 shown in the previous figure. In the embodiment of figure 10, crossing device 70 has been withdrawn from true lumen 30 of artery 20. With reference to figure 10, it will be appreciated that guidewire 60 remains in the position formerly occupied by crossing device 70.

The position of guidewire 60 shown in figure 10 may be achieved using crossing device 70. Guidewire 60 may be positioned, for example, by first placing crossing device 70 in the position shown in the previous figure, then advancing guidewire 60 through lumen 122 defined by shaft 72 of crossing device 70. Alternately, guidewire 60 may be disposed within lumen 122 while crossing device 70 is advanced beyond occlusion 36.

With guidewire 60 in the position shown in figure 10, guidewire 60 may be used to direct other devices between occlusion 36 and adventitia 24. For example, a catheter may be advanced over guidewire 60 until the distal end of the catheter extends between an occlusion and the adventitia. After reaching this location, the catheter may be used to dilate the tissue surrounding the catheter. Examples of catheters that may be used to dilate tissue include inflatable member catheters and atherectomy catheters.

Figure 11 is an additional view of artery 20 and guidewire 60 shown in the previous figure. In the embodiment of figure 11, an orienting device 100 has been advanced over guidewire 60. Orienting device 100 includes a distal shaft 102 comprising an outer wall 128 defining a central lumen 104. A first aperture 130 and a second aperture 132 are also defined by outer wall 128. In the embodiment of figure 11, first aperture 130 and second aperture 132 are both in fluid communication with central lumen 104.

In the embodiment of figure 11, orienting device 100 has been positioned so that first aperture 130 opens toward intima 26 of artery 20 and second aperture 132 opens toward adventitia 24. In the embodiment of figure 11, first aperture 130 and second aperture 132 are longitudinally separated from one another. Orienting device 100 includes a first radiopaque marker that is located between first aperture 130 and second aperture 132. A second radiopaque marker of orienting device 100 is located distally of second aperture 132.

Figure 12 is an additional view of artery 20 and orienting device 100 shown in the previous figure. In the embodiment of figure 12, guidewire 60 has been withdrawn leaving orienting device 100 in the position shown in figure 12. With reference to figure 12, it will be appreciated that orienting device 100 extends beyond occlusion 36. In figure 12, occlusion 36 is shown blocking true lumen 30. Occlusion 36 divides true lumen 30 into a proximal segment 32 and a distal segment 34. When an orienting device in accordance with

some embodiments disclosed herein is advanced between the adventitia and the intima of an artery, the orienting device may be used to direct a re-entry device toward true lumen 30. Fluid communication between proximal segment 32 and distal segment 34 may be achieved by re-entering the true lumen with the re-entry device.

Figure 13 is an additional view of artery 20 and orienting device 100 shown in the previous figure. In the embodiment of figure 13, a re-entry device 80 has been advanced into central lumen 104 of orienting device 100. A distal end 132 of re-entry device 80 has been advanced through first aperture 130 and can be seen residing in true lumen 30.

After re-entry device 80 is positioned as shown in figure 13, orienting device 100 may be withdrawn leaving re-entry device 80 in the position shown in figure 13. Devices such as inflatable member angioplasty catheters and atherectomy catheters may then be advanced over re-entry device 80. In this way, these devices may be used in conjunction with re-entry device 80 to establish a blood flow path between proximal segment 32 of true lumen 30 and distal segment 34 of true lumen 30. This path allows blood to flow around occlusion 36.

Figure 14 is an enlarged cross-sectional view of orienting device 100 shown in the previous figure. Orienting device 100 includes a distal shaft 102 comprising an outer wall 128 defining a central lumen 104. Outer wall 128 defines a first aperture 130 and a second aperture 132 that are both in fluid communication with central lumen 104. In the embodiment of Figure 14, first aperture 130 extends away from central lumen 104 in a first direction that is represented by a first arrow AA in Figure 14. Second aperture 132 extends away from central lumen 104 in a second direction that is represented by a second arrow AB in Figure 14. In Figure 14, first arrow AA and second arrow AB extend in generally opposite directions. In figure 14, first arrow AA and second arrow AB are directed about 180 degrees away from one another.

In the embodiment of Figure 14, first aperture 130 and second aperture 132 are longitudinally separated from one another. Orienting device 100 includes a first radiopaque marker 134A that is located between first aperture 130 and second aperture 132. A second radiopaque marker 134B of orienting device 100 is located distally of second aperture 132.

A re-entry device 80 is disposed in central lumen 104 of orienting device 100. In the embodiment of Figure 14A, first radiopaque marker 134A, second radiopaque marker 134B and re-entry device 80 comprise radiopaque materials. Because of the radiopaque nature of their materials of construction, first radiopaque marker 134A, second radiopaque marker 134B, and re-entry device 80 will all be visible on a fluoroscopic display during a

fluoroscopic procedure. The relative location of these radiopaque elements on the fluoroscopic display can be used to direct the distal end of re-entry device 80 through a selected aperture in orienting device 100.

Figure 15 is a stylized plan view showing orienting device 100 shown in the previous figure. In figure 15, a distal portion of re-entry device 80 can be seen extending through first aperture 130. First aperture 130 and second aperture 132 both fluidly communicate with central lumen 104 of orienting device 100. Orienting device 100 includes a first radiopaque marker 134A that is located between first aperture 130 and second aperture 132. A second radiopaque marker 134B of orienting device 100 is located distally of second aperture 132.

Orienting device 100 comprises an orienting element 120 that is fixed to a distal shaft 102. Orienting element 120 comprises an inflatable member 126. When inflatable member 126 of orienting element 120 is inflated between the adventicia and the intima of a blood vessel, orienting device 100 will orient itself within the blood vessel so that either first aperture 130 or second aperture 132 opens toward a true lumen of the artery. The physician may select the aperture opening toward the true lumen, for example, using the fluoroscopic methods described herein. The physician may then insert the distal end of re-entry device 80 through the selected aperture.

Figure 16 is a perspective view of an orienting device 200. Orienting device 200 comprises a distal shaft 202, a proximal shaft 92 and an intermediate shaft 82 that extends between distal shaft 202 and proximal shaft 92. Orienting device 200 includes an orienting element 220 that is coupled to a distal shaft 202. In the embodiment of figure 21, orienting element 220 comprises an inflatable member 226 that is fixed to distal shaft 202. Inflatable member 226 may be fixed to distal shaft 202, for example, at a proximal waist 246A, at a distal waist 246B, at the top of the inflatable member 226, and at the bottom of the inflatable member.

Orienting element 220 comprises a first portion 206 and a second portion 208. First portion 206 of orienting element 220 extends in a first direction away from distal shaft 202. Second portion 208 of orienting element 220 extends away from distal shaft 202 in a second direction that is generally opposite the first direction.

A hub 236 is fixed to the proximal end of proximal shaft 92. Hub 236 includes a proximal port 238. Proximal port 238 fluidly communicates with an interior of inflatable member 226 via inflation lumens defined by distal shaft 202, intermediate shaft 82, and proximal shaft 92. Inflatable member 226 may be inflated by injecting an inflation media

into proximal port 238. Examples of inflation media that may be suitable in some applications include saline, carbon dioxide, or nitrogen. In some useful embodiments, inflatable member 226, distal shaft 202, intermediate shaft 82, and proximal shaft 92 comprise thermoplastic materials. Examples of thermoplastic materials that may be suitable in some applications include Nylon, Pebax, or P.E.T.

A first aperture 230 is disposed on a first side of orienting element 220. When inflatable member 226 of orienting element 220 is inflated between the adventicia and the intima of a blood vessel, orienting device 200 will orient itself within the blood vessel so that first aperture 230 either opens toward the true lumen of the artery or opens 180 degrees away from the true lumen of the artery. A second aperture is disposed on a second side of orienting element 220. Second aperture is not visible in figure 16. First aperture 230 is disposed on a first side of orienting element 220 and the second aperture is disposed on a second side of orienting element that is generally opposite the first side.

Figure 17 is a plan view showing an additional exemplary orienting device 300. Orienting device 300 of figure 17 comprises an orienting element 320 coupled to a distal shaft 302. In the embodiment of figure 17, orienting element 320 comprises a first inflatable member 322 and a second inflatable member 324. In the embodiment of Figure 17, first inflatable member 322 and second inflatable member 324 are both formed from extruded portions of an outer wall 328 of distal shaft 302. Outer wall 328 defines a first aperture 330 and a second aperture 332. With reference to figure 17, it will be appreciated that first aperture 330 and second aperture 332 are both disposed between first inflatable member 322 and second inflatable member 324.

Figure 18 is a stylized perspective view showing a portion 340 of orienting device 300 shown in the previous figure. Portion 340 is created by cutting orienting device 300 along cutting plane A-A and cutting plane B-B shown in the previous figure.

Orienting device 300 comprises an orienting element 320 that is coupled to a distal shaft 302. Orienting element 320 comprises a first inflatable member 322 and a second inflatable member 324. First inflatable member 322 of orienting element 320 extends in a first direction away from distal shaft 302. Second inflatable member 324 of orienting element 320 extends away from distal shaft 302 in a second direction that is generally opposite the first direction.

With reference to figure 18, it will be appreciated that first inflatable member 322 extends away from outer wall 328 in a first direction that is represented by an arrow labeled OD. With continuing reference to figure 18, it will be appreciated that second inflatable

member 324 extends way from distal shaft 302 in a second direction that is generally opposite the first direction. In figure 18, the second direction is represented by an arrow labeled SD.

With reference to Figure 18, it will be appreciated that an outer wall 328 of distal shaft 302 defines a first aperture 330 and a second aperture 332. First aperture 330 extends away from central lumen 304 in a third direction that is represented by an arrow labeled TD. With continuing reference to figure 18, it will be appreciated that second aperture 332 extends away from central lumen 304 in a forth direction that is generally opposite the third direction. In figure 18, the fourth direction is represented by an arrow labeled FD.

With reference to figure 18, it will be appreciated that first aperture 330 and second aperture 332 are both disposed between first inflatable member 322 and second inflatable member 324. First aperture 330 and second aperture 332 both fluidly communicate with a central lumen 304 defined by distal shaft 302. First aperture 330 and second aperture 332 are generally oriented at a right angle to a plane P defined by first inflatable member 322 and second inflatable member 324 of orienting element 320.

Figure 19 is a stylized cross-sectional view showing orienting device 300 shown in the previous figure. With reference to Figure 19, it will be appreciated that distal shaft 302 defines a central lumen 304, a first planetary lumen 342, a second planetary lumen 344. The planetary lumens are defined in part by an outer wall 328 of distal shaft 302. Outer wall 328 also defines a first aperture 330 and a second aperture 332. First aperture 330 and second aperture 332 both fluidly communicate with central lumen 304.

Orienting device 300 comprises an orienting element 320 that includes a first inflatable member 322 and a second inflatable member 324. In the embodiment of Figure 19, first inflatable member 322 is formed of an extruded portion of outer wall 328 of distal shaft 302. First inflatable member 322 defines an interior that is in fluid communication with first planetary lumen 342. In the embodiment of Figure 19, first inflatable member 322 and distal shaft 302 are monolithic. As shown in Figure 19, first inflatable member 322 and outer wall 328 of distal shaft 302 are seamlessly formed from a single piece of material. With reference to Figure 19, it will be appreciated that second inflatable member 324 defines an interior that is in fluid communication with second planetary lumen 344. In the embodiment of Figure 19, second inflatable member 324 comprises an extruded portion of outer wall 328 of distal shaft 302.

One potential advantage of creating an orienting element from a monolithic tube is the elimination of fixation points between the orienting element and catheter shaft thus

reducing processing steps and manufacturing cost. Another potential advantage is the reduction of fixation points between the orienting element and catheter shaft which may also reduce the distal diameter of the catheter by eliminating areas of overlapping material. Another potential advantage may include the reduction of potential failure points through the elimination of fixation points (e.g. thermal or adhesive bonds) between the orienting element and the catheter shaft.

First inflatable member 322 of orienting element 320 extends in a first direction away from distal shaft 302. Second inflatable member 324 of orienting element 320 extends away from distal shaft 302 in a second direction that is generally opposite the first direction.

In the embodiment of figure 19, orienting element 320 is assuming a deployed shape. Also in the embodiment of figure 19, first inflatable member 322 and second inflatable member 324 are both in a generally inflated state. With reference to figure 19, it will be appreciated that first inflatable member 322 and second inflatable member 324 define a plane P. With continuing reference to figure 19, it will be appreciated that orienting element 320 has a first width WA and first thickness TA. In the embodiment of figure 19, first width WA is greater than first thickness TA when orienting element 320 is assuming a deployed shape.

In some useful embodiments, an aspect ratio of first width WA to first thickness TA is greater than about one when orienting element 320 is assuming a deployed shape. In some particularly useful embodiments, the aspect ratio of first width WA to first thickness TA is greater than about two when orienting element 320 is assuming a deployed shape. In some especially useful embodiments, the aspect ratio of first width WA to first thickness TA is greater than about three when orienting element 320 is assuming a deployed shape.

Figure 20 is an additional stylized cross-sectional view showing orienting device 300 shown in the previous figure. In the embodiment of figure 20, orienting element 320 is assuming a generally collapsed shape and the inflatable members are in a substantially deflated state. When the inflatable members are deflated, orienting element 320 may assume various collapsed and/or folded shapes. In the embodiment of figure 20, orienting element 320 has a second width WB.

A deployed shape of orienting element 320 is shown with dotted lines in figure 20. With reference to figure 20, it will be appreciated that orienting element 320 has a first width WA that is greater than second width WB when orienting element 320 is assuming a deployed shape.

Figure 21 is a plan view showing an additional exemplary orienting device 700. Orienting device 700 of figure 21 comprises an orienting element 720 coupled to a distal shaft 702. In the embodiment of figure 21, orienting element 720 comprises a first inflatable member 722 and a second inflatable member 724. In the embodiment of Figure 21, first inflatable member 722 and second inflatable member 724 are both formed from extruded portions of an outer wall 728 of distal shaft 702. Outer wall 728 defines a first aperture 730 and a second aperture 732. With reference to figure 21, it will be appreciated that first aperture 730 and second aperture 732 are both disposed between first inflatable member 722 and second inflatable member 724.

With reference to figure 21, it will be appreciated that first inflatable member 722 has a first length LA and second inflatable member 724 has a second length LB. In the embodiment of figure 21, second length LB is greater than first length LA. In one useful method, first inflatable member 722 and second inflatable member 724 are both inflated with a radiopaque inflation media. When this is the case, a physician may use fluoroscopic visualization techniques to determine the orientation of orienting device 700 by observing first inflatable member 722 and second inflatable member 724 on the fluoroscopic display.

From the foregoing, it will be apparent to those skilled in the art that the present invention provides, in exemplary non-limiting embodiments, devices and methods for the treatment of chronic total occlusions. Further, those skilled in the art will recognize that the present invention may be manifested in a variety of forms other than the specific embodiments described and contemplated herein. Accordingly, departures in form and detail may be made without departing from the scope and spirit of the present invention as described in the appended claims.

CLAIMS

What is claimed is:

1. An apparatus for facilitating treatment via a vascular wall defining a vascular lumen containing an occlusion therein, the apparatus comprising:
a first intravascular device having a distal portion, the distal portion including at least one aperture, at least one radiopaque marker, and at least one orienting element.
2. The apparatus of claim 1, wherein the at least one aperture includes two apertures, and wherein the first aperture is located proximal the second aperture.
3. The apparatus of claim 2, wherein the at least one radiopaque marker is located distal the first aperture.
4. The apparatus of claim 2, wherein the at least one radiopaque marker comprises a first radiopaque marker located between the first aperture and the second aperture, and a second radiopaque marker located distal the second aperture.
5. The apparatus of claim 4, further including a fluoroscopic display, and wherein the reentry device is configured to be visible on the fluoroscopic display.
6. The apparatus of claim 1, further comprising a reentry device rotatable within the first intravascular device and configured to advance through the at least one aperture.
7. The apparatus of claim 1, wherein the at least one orienting element comprises an inflatable member configured to orient the first intravascular device after being inflated.
8. The apparatus of claim 1, wherein the at least one orienting element comprises two inflatable members, configured to orient the first intravascular device after being inflated.

9. The apparatus of claim 8, wherein the first inflatable member extends from a shaft of the first intravascular device in a first direction, the second inflatable member extends from the shaft in a second direction substantially opposite the first direction.

10. The apparatus of claim 9, wherein the at least one aperture includes two apertures, and wherein the first aperture is located proximal the second aperture.

11. The apparatus of claim 10, wherein the first aperture extends in a third direction through a wall of the first intravascular device, and the second aperture extends in a fourth direction through a wall of the first intravascular device.

12. The apparatus of claim 11, wherein the fourth direction is generally opposite the third direction.

13. The apparatus of claim 11, wherein the fourth direction is generally perpendicular to the first direction and the second direction.

14. The apparatus of claim 10, wherein the first aperture and the second aperture are longitudinally offset from one another.

15. The apparatus of claim 9, wherein:
the first intravascular device has a first width and a first thickness when the two inflatable members are in a substantially inflated state; and
the first intravascular device has a second width when the two inflatable members are in a substantially deflated state.

16. The apparatus of claim 15, wherein the first width is greater than the second width.

17. The apparatus of claim 15, wherein the first width is greater than the first thickness.

18. The apparatus of claim 9, wherein the first and second inflatable members comprise extruded portions of an outer wall of the shaft.

19. The apparatus of claim 9, wherein:
the shaft defines first and second planetary lumens; and
the first and second inflatable members are in fluid communication with the first and second planetary lumens respectively.

20. The apparatus of claim 9, wherein the first inflatable member has a first length and the second inflatable member has a second length that is greater than the first length.

21. An apparatus for facilitating treatment via a vascular wall defining a vascular lumen containing an occlusion therein, the apparatus comprising:
an orienting device having a distal portion, the distal portion including a first aperture located proximal a second aperture, at least one radiopaque marker located distal the first aperture, and an orienting element including two inflatable members.

22. The apparatus of claim 21, wherein the at least one radiopaque marker is two radiopaque markers, and wherein the first radiopaque marker is located between the first and second apertures, and the second radiopaque marker is located distal the second aperture.

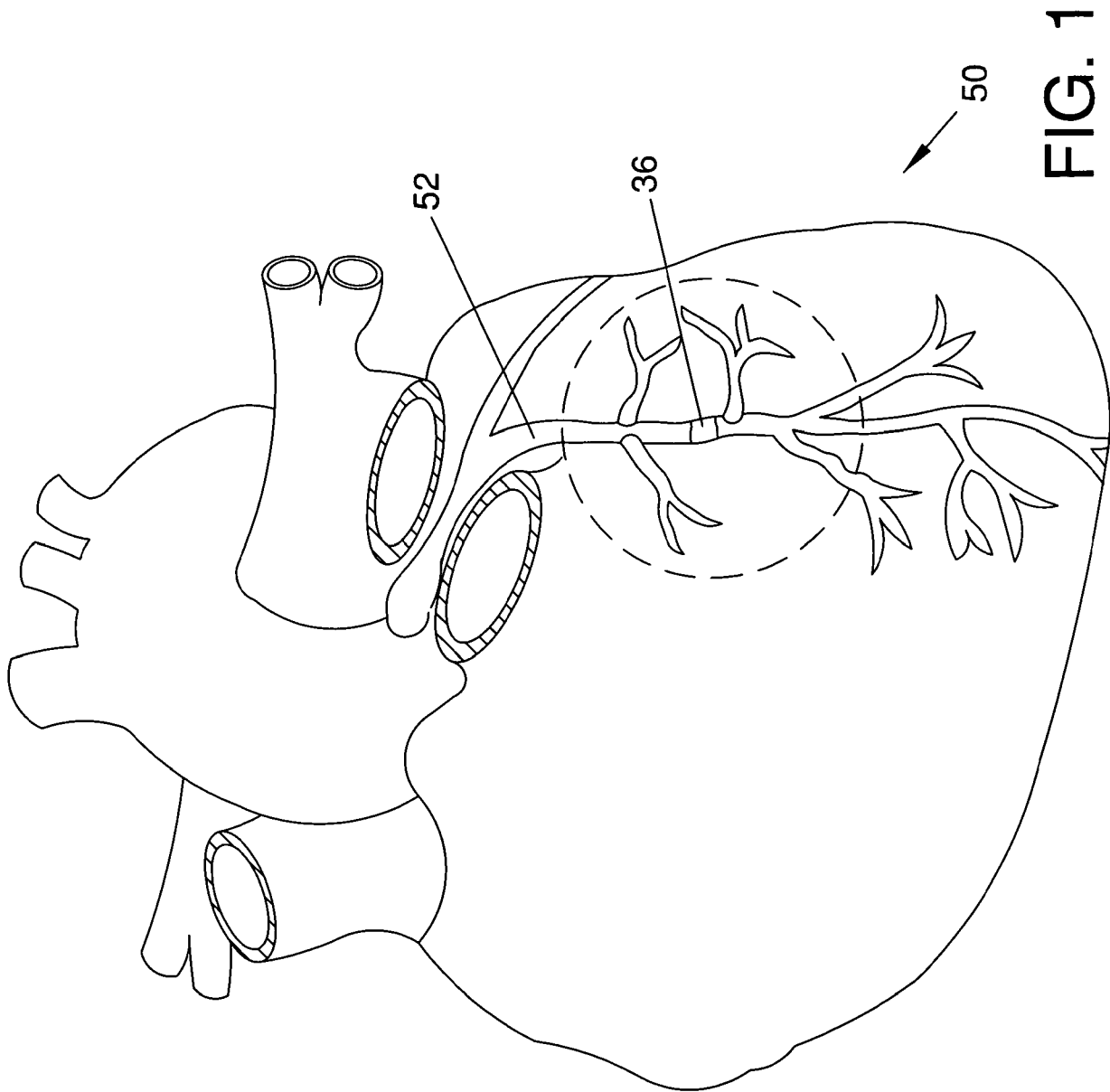
23. The apparatus of claim 22, further including a shaft, and wherein the first inflatable member extends from the shaft of the orienting device in a first direction, the second inflatable member extends from the shaft in a second direction substantially opposite the first direction.

24. The apparatus of claim 23, wherein the first aperture extends in a third direction through a wall of the orienting device, and the second aperture extends in a fourth direction through a wall of the orienting device, and wherein the fourth direction is generally opposite the third direction.

25. The apparatus of claim 24, wherein the orienting device has a first width and a first thickness when the two inflatable members are in a substantially inflated state, and the orienting device has a second width when the two inflatable members are in a substantially deflated state.

26. The apparatus of claim 24, wherein the third and fourth directions are generally perpendicular to the first and second directions.

27. The apparatus of claim 21, further including a reentry device having a body and a distal tip, the reentry device being rotatable within the distal portion of the orienting device and configured to advance through the two apertures.



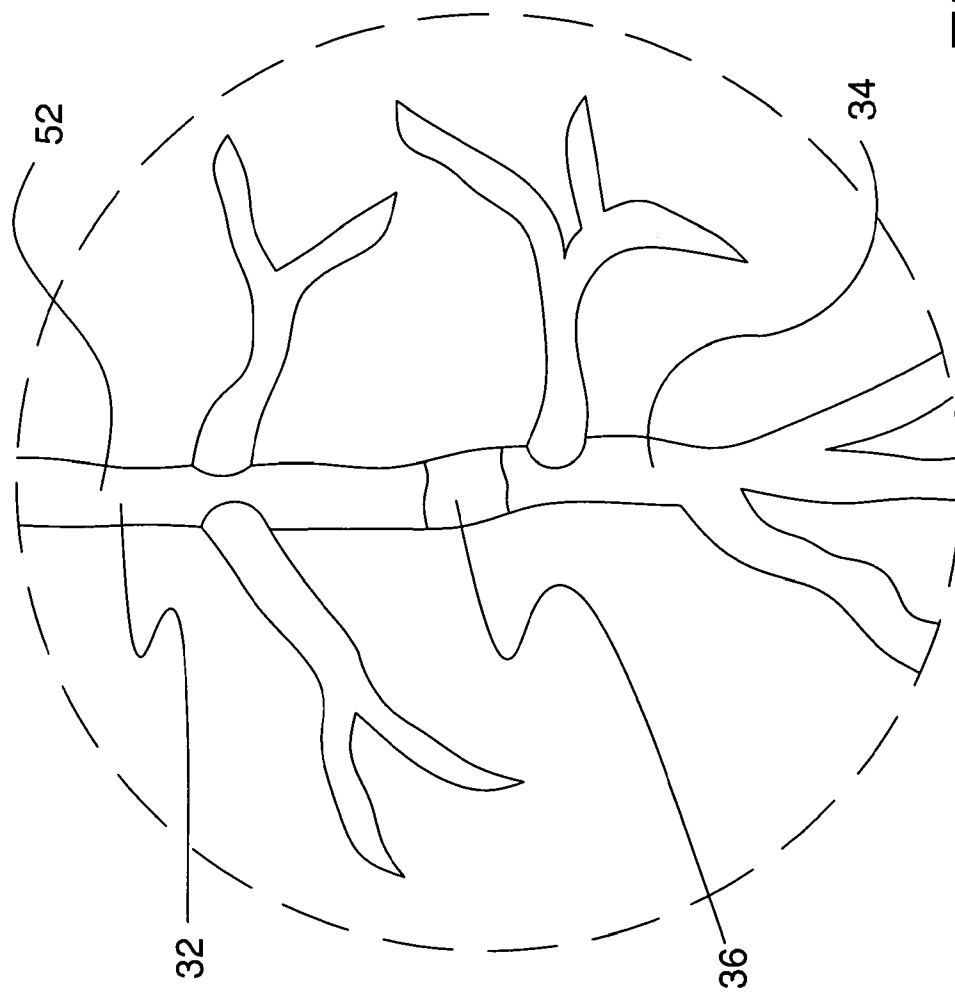


FIG. 2

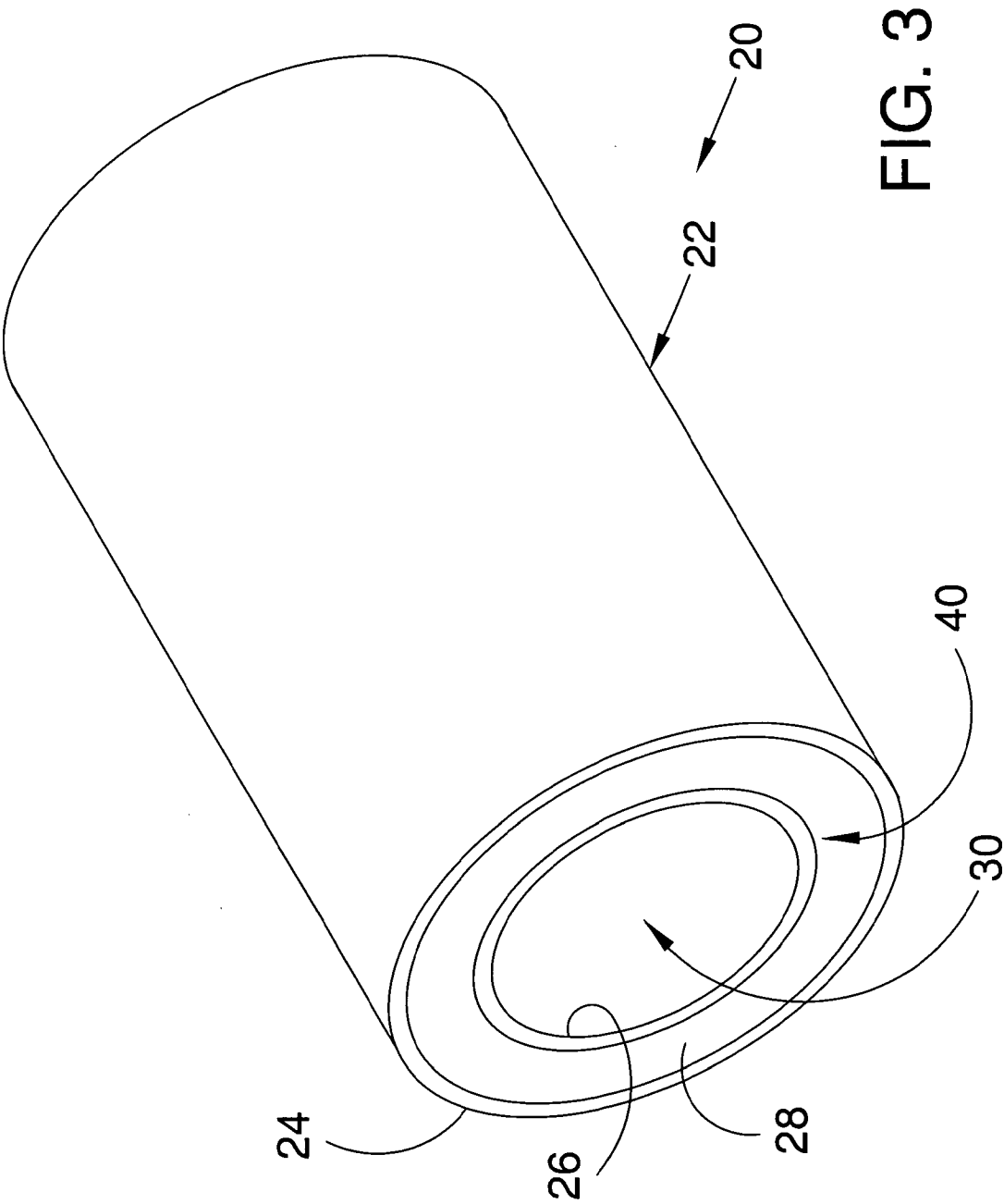


FIG. 3

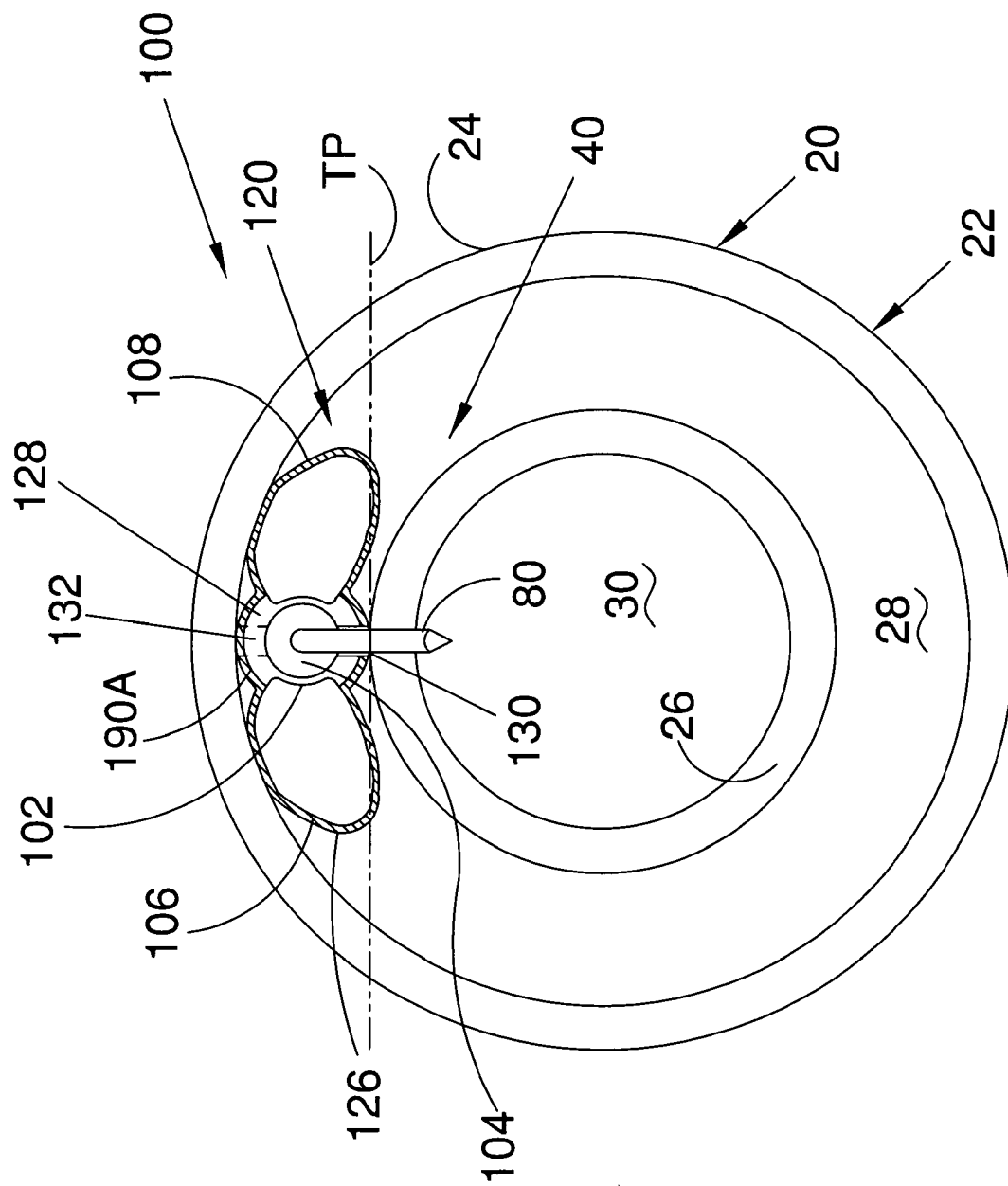


FIG. 4

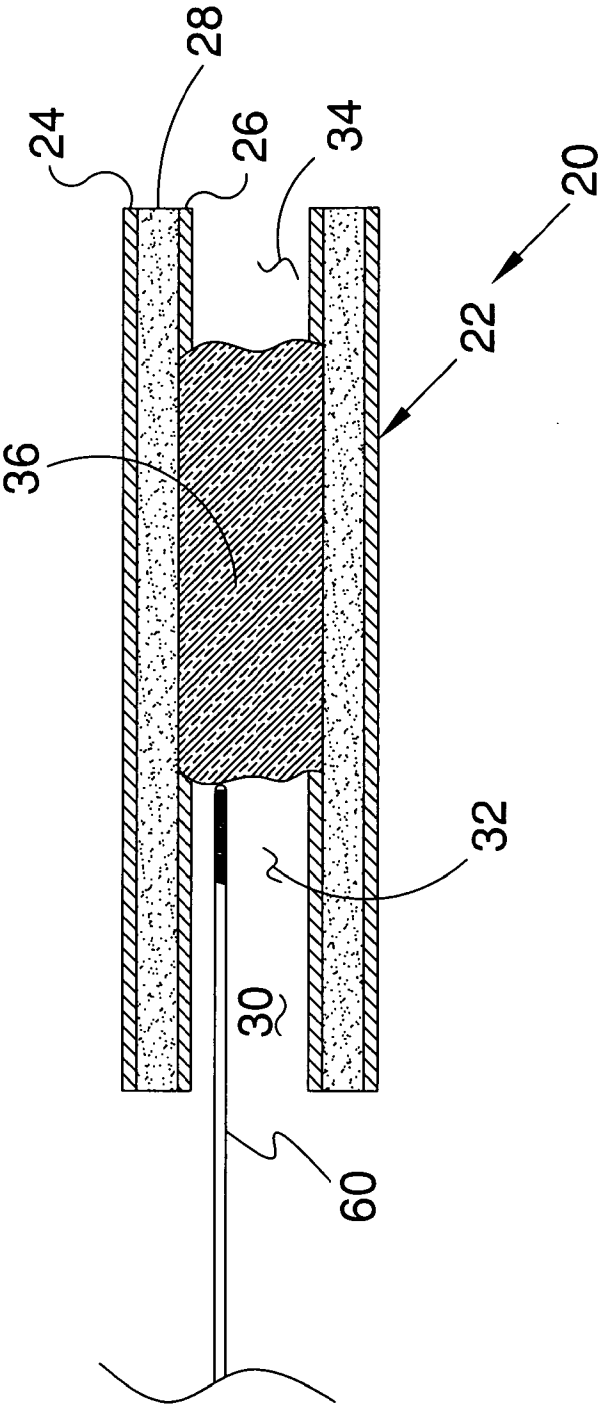


FIG. 5

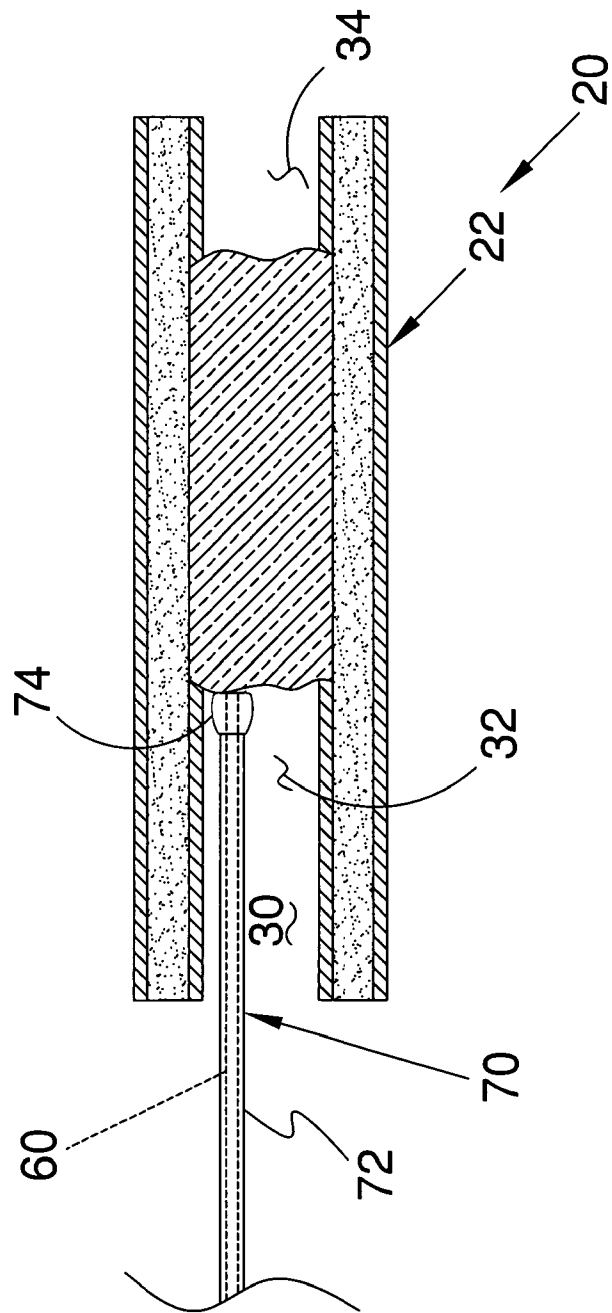


FIG. 6

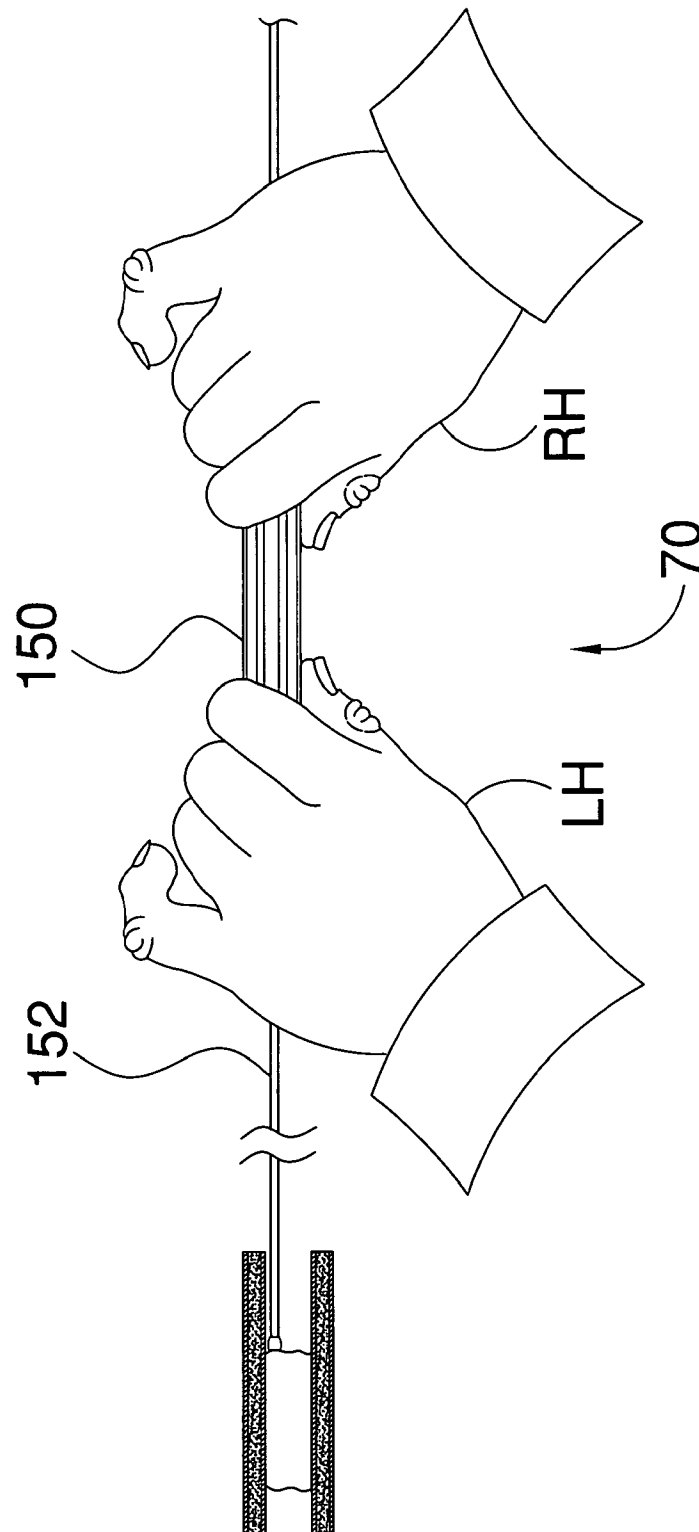


FIG. 7

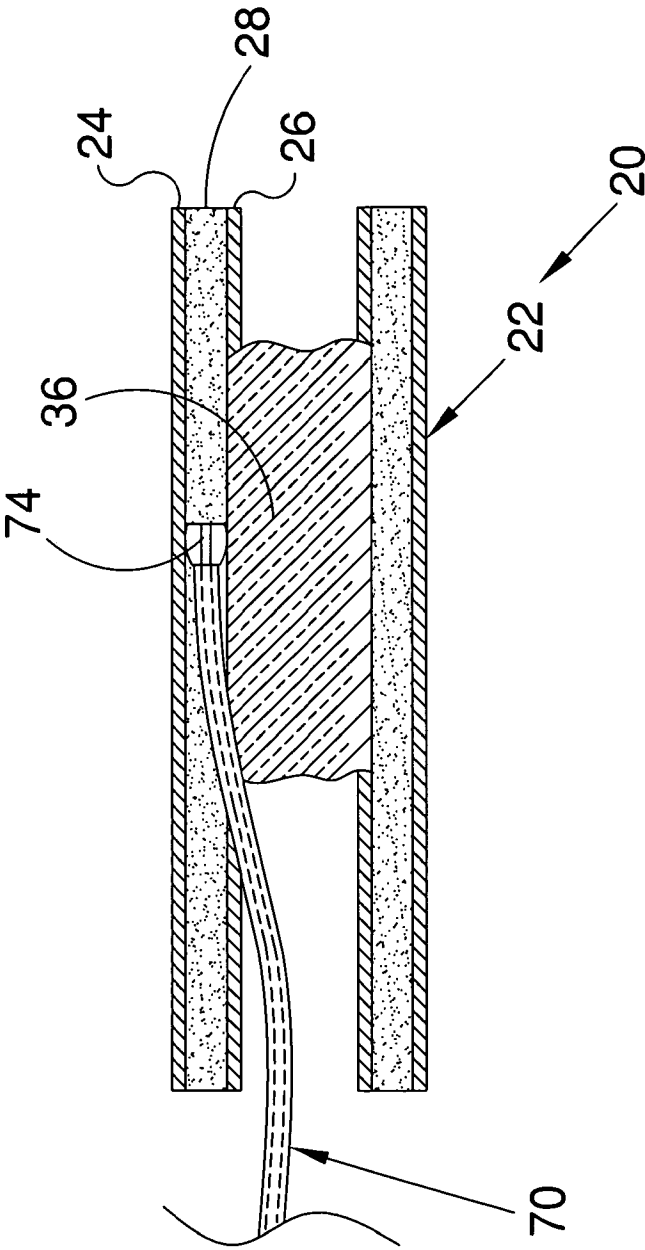


FIG. 8

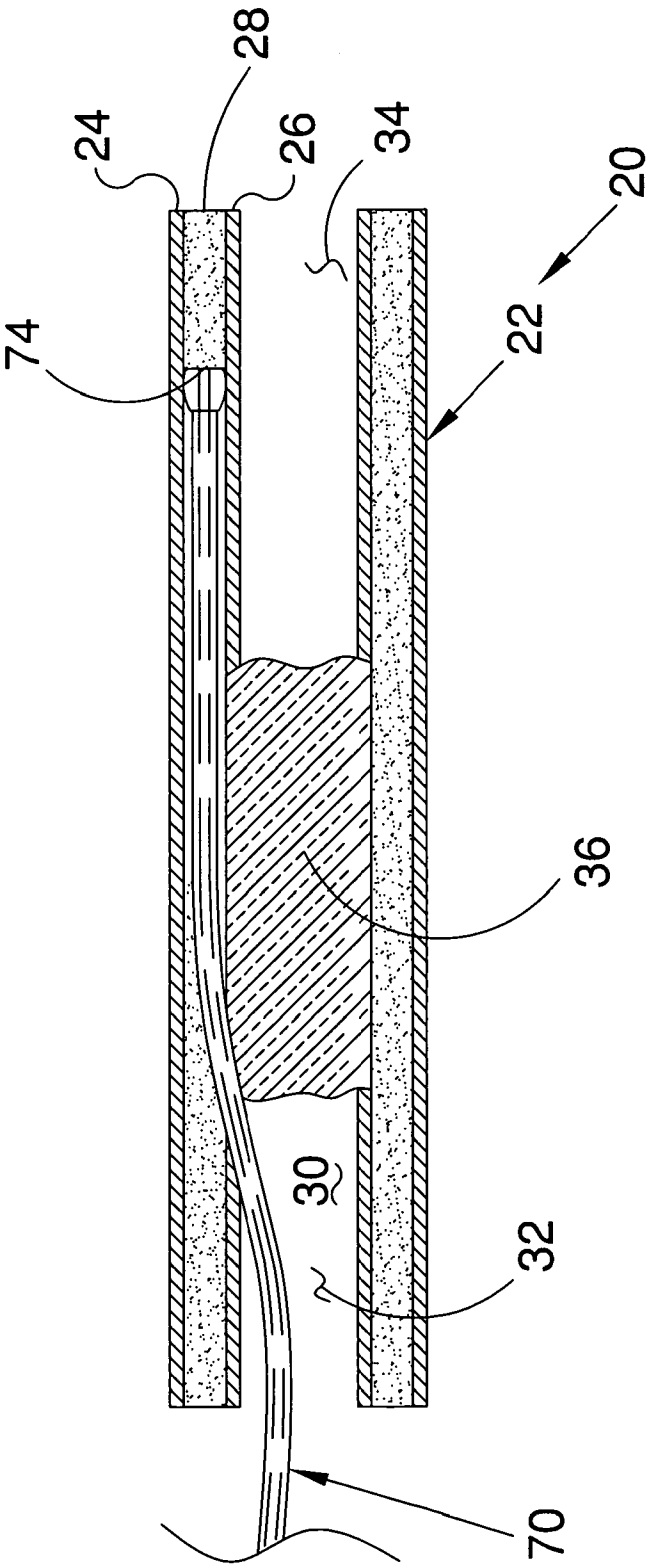


FIG. 9

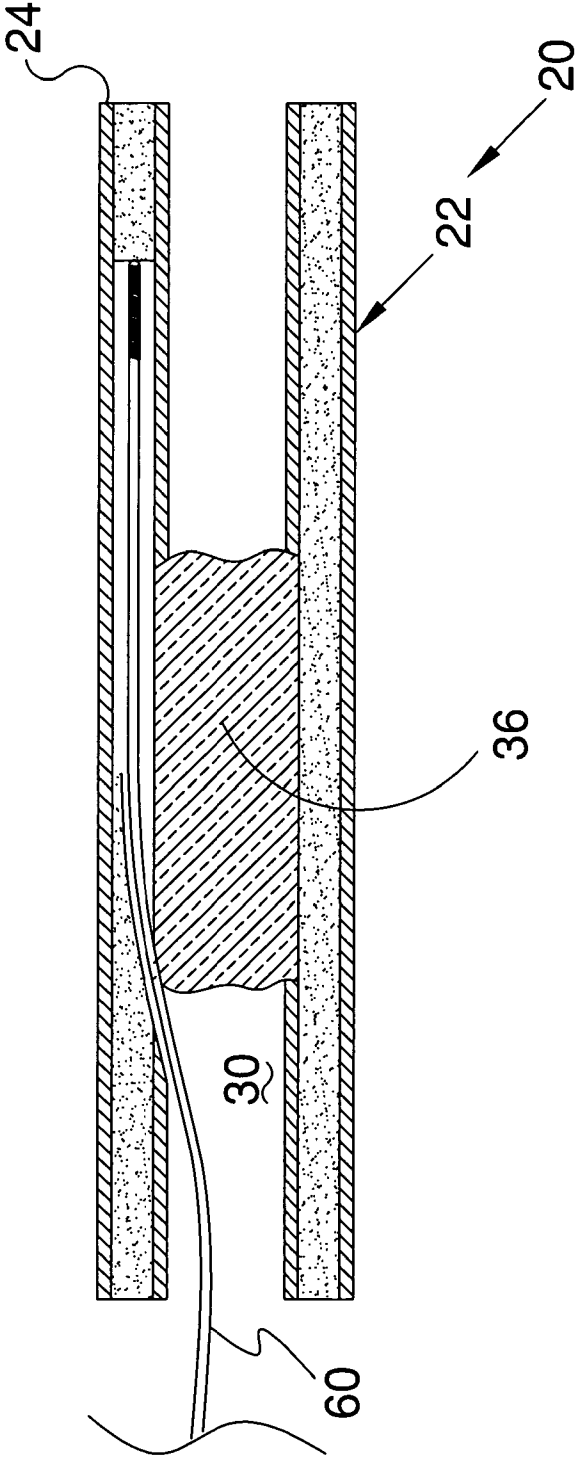


FIG. 10

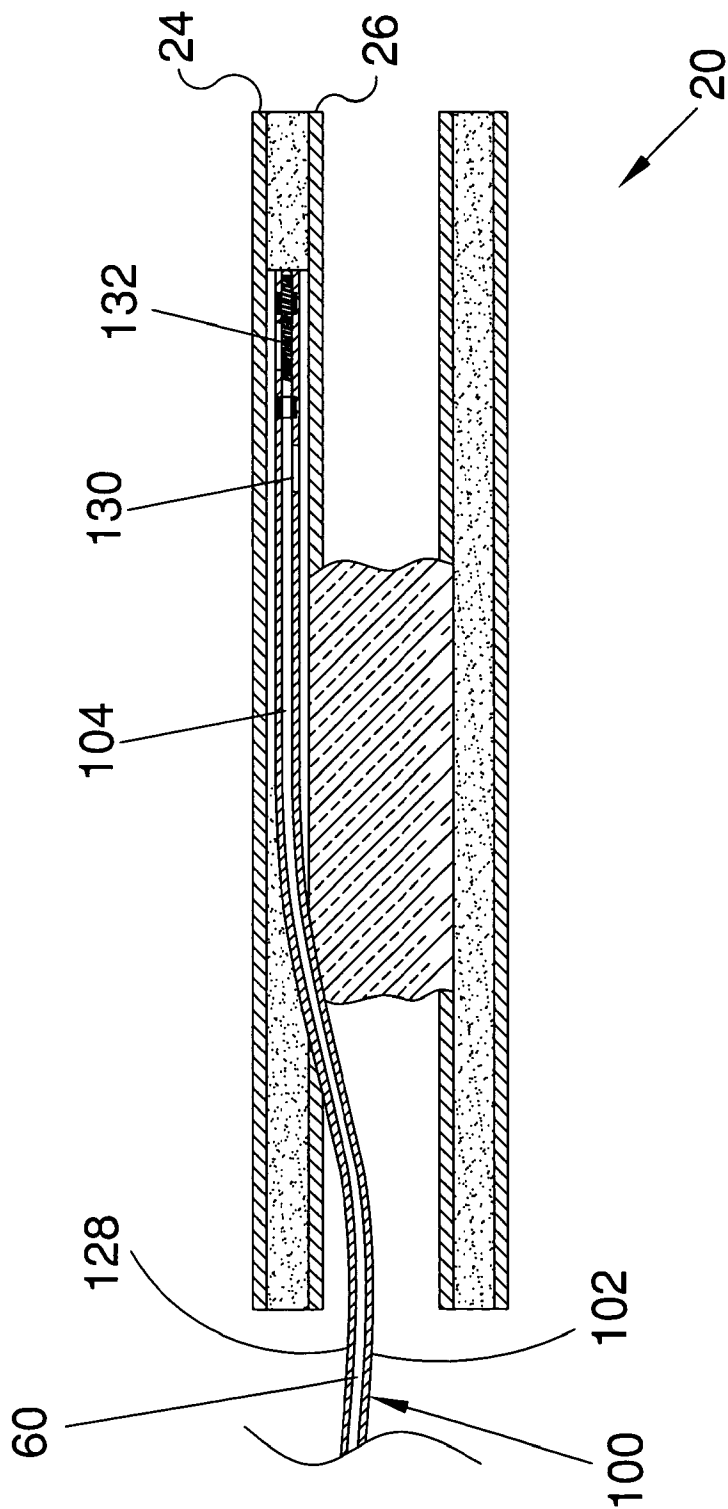


FIG. 11

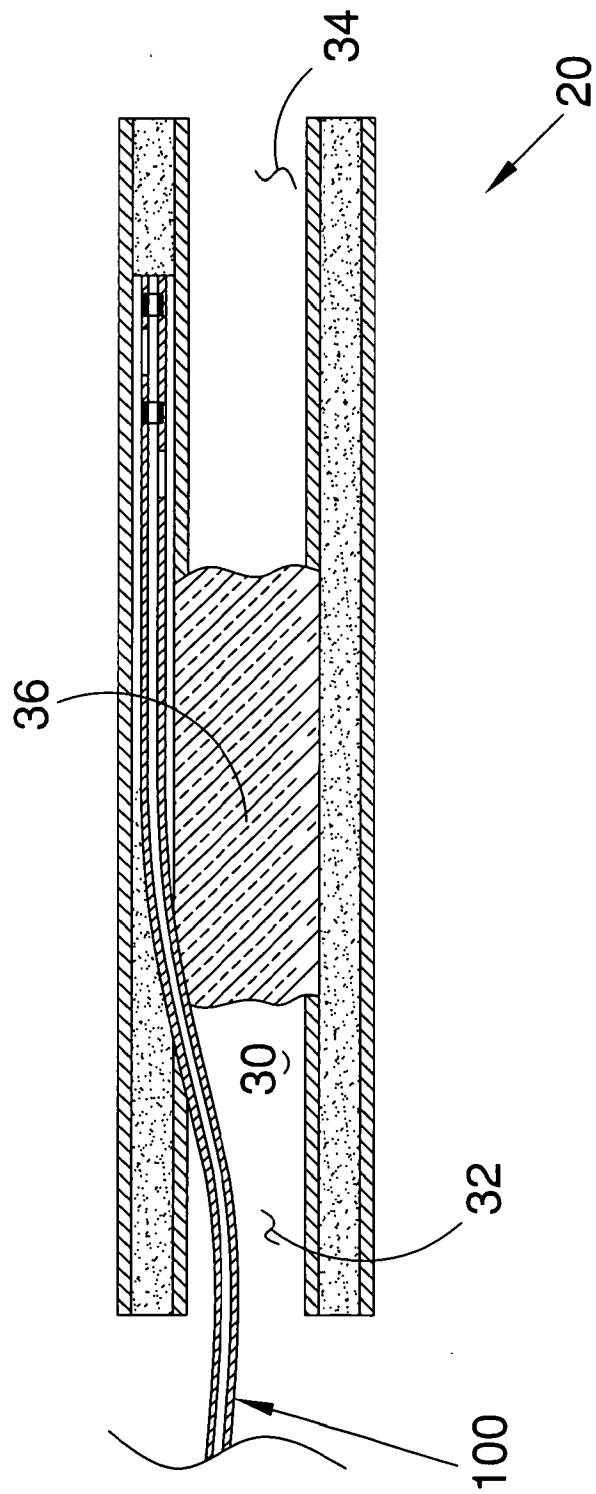


FIG. 12

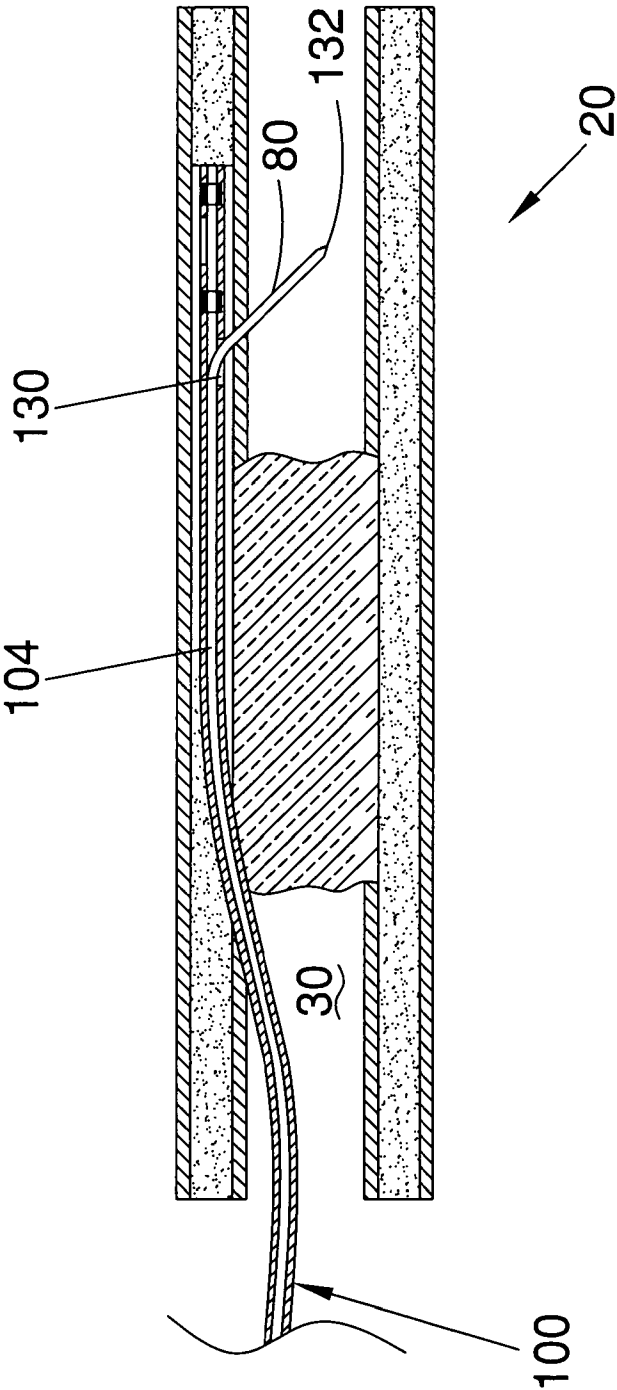


FIG. 13

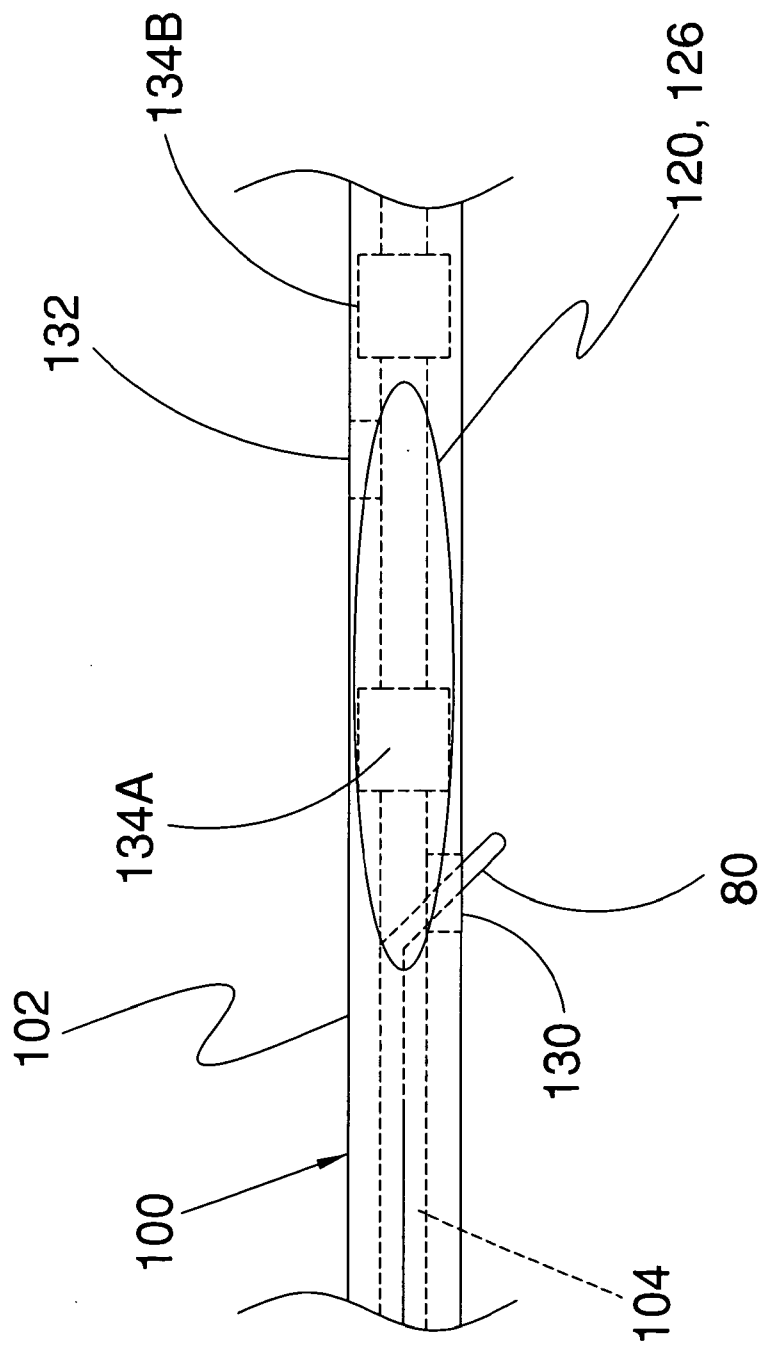


FIG. 15

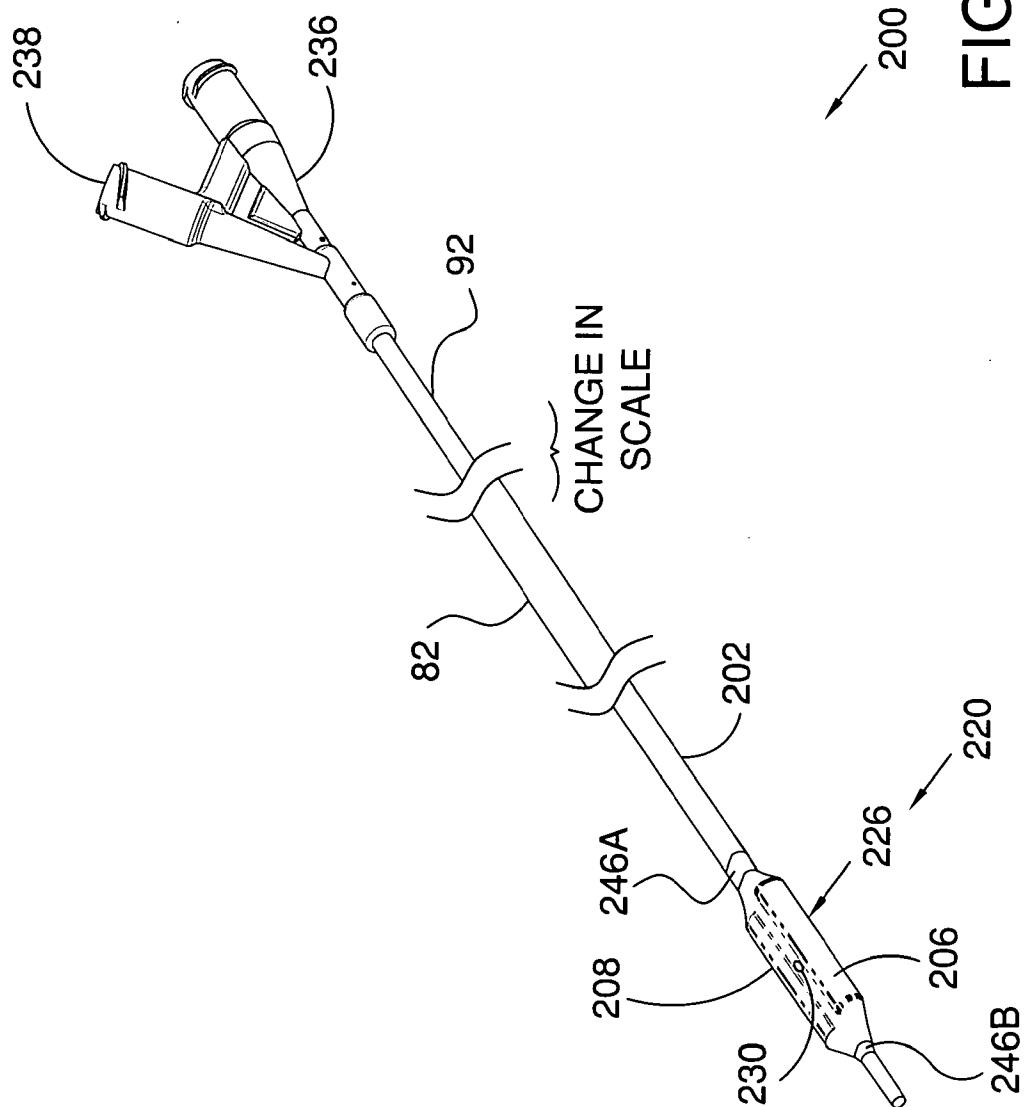


FIG. 16

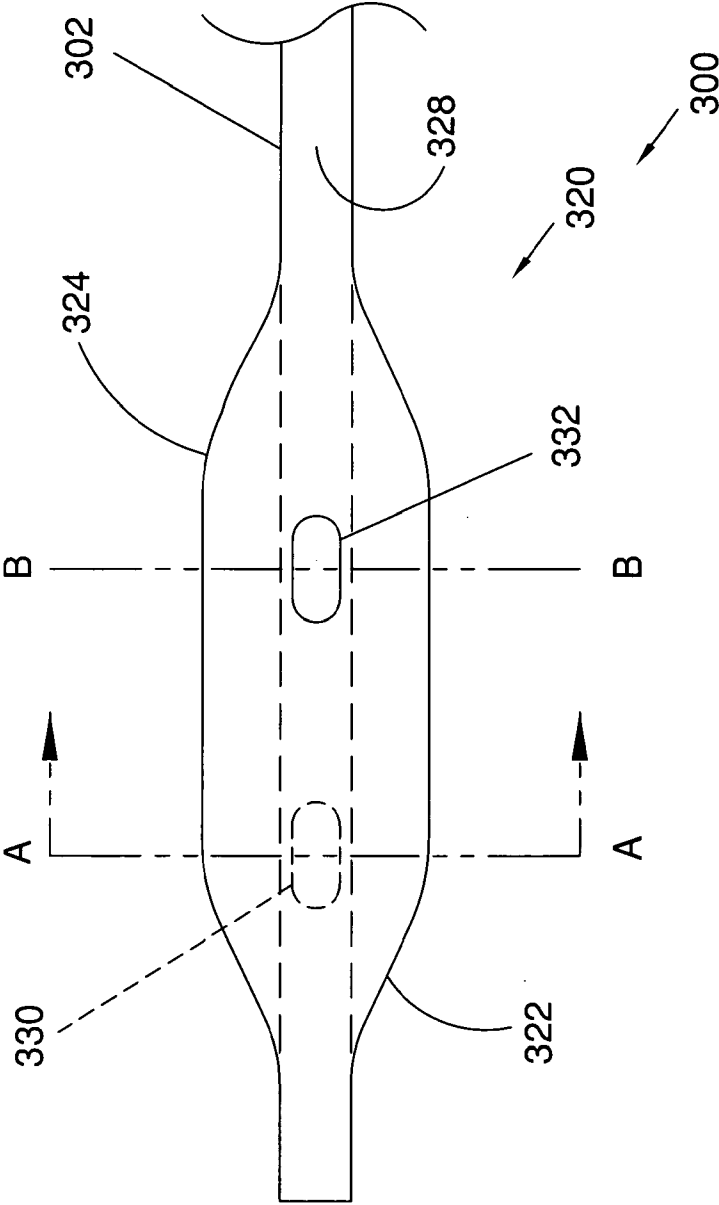
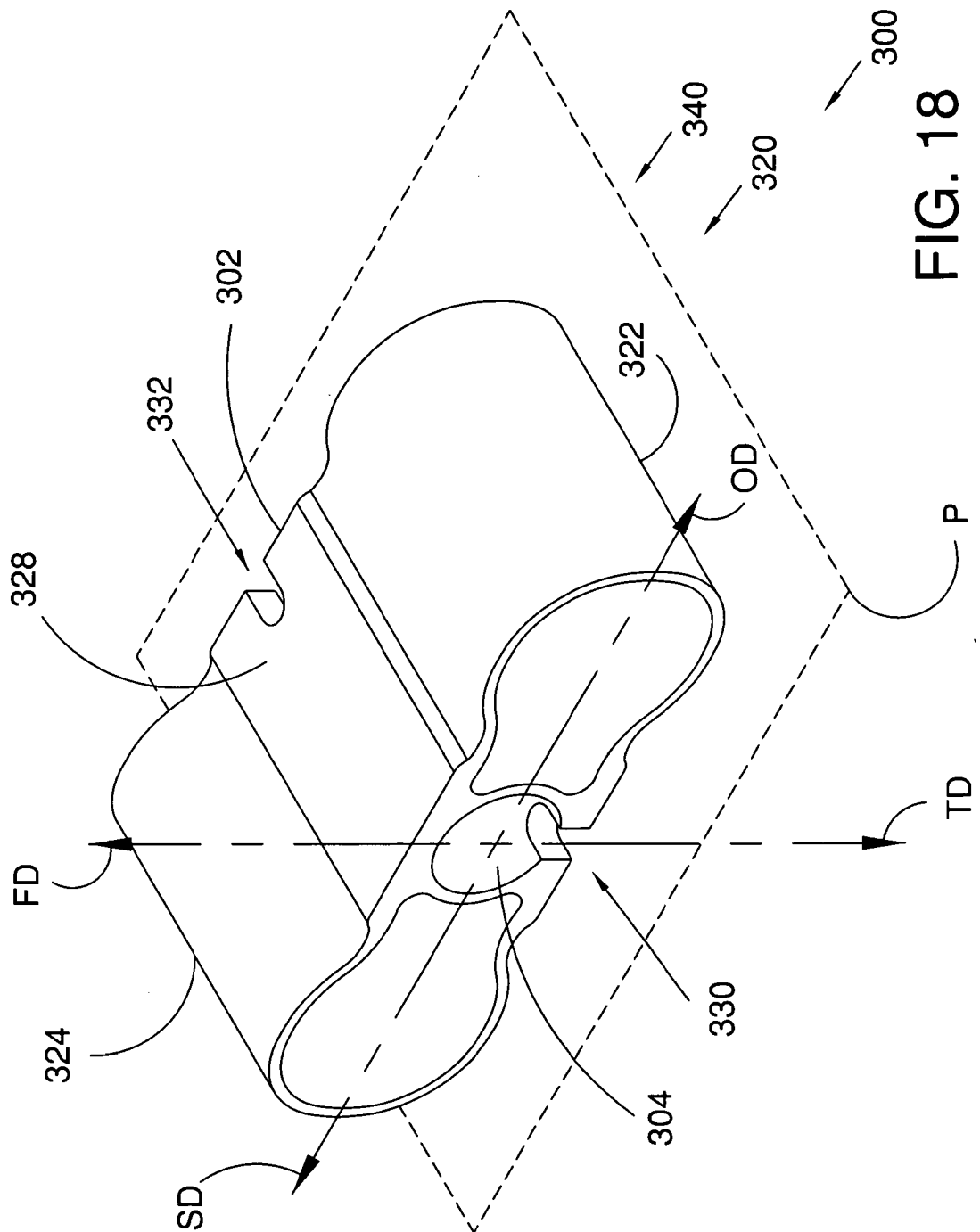


FIG. 17



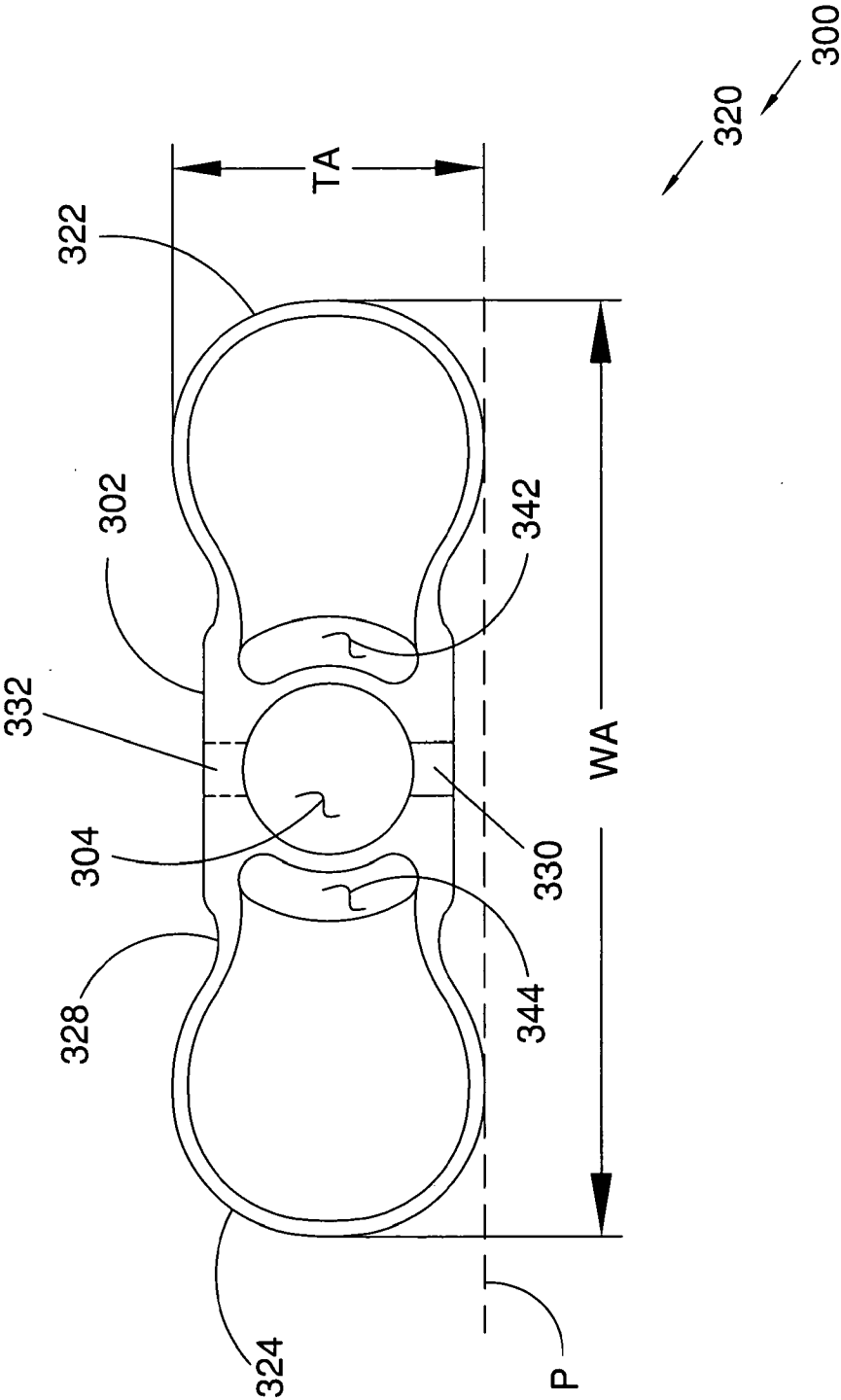


FIG. 19

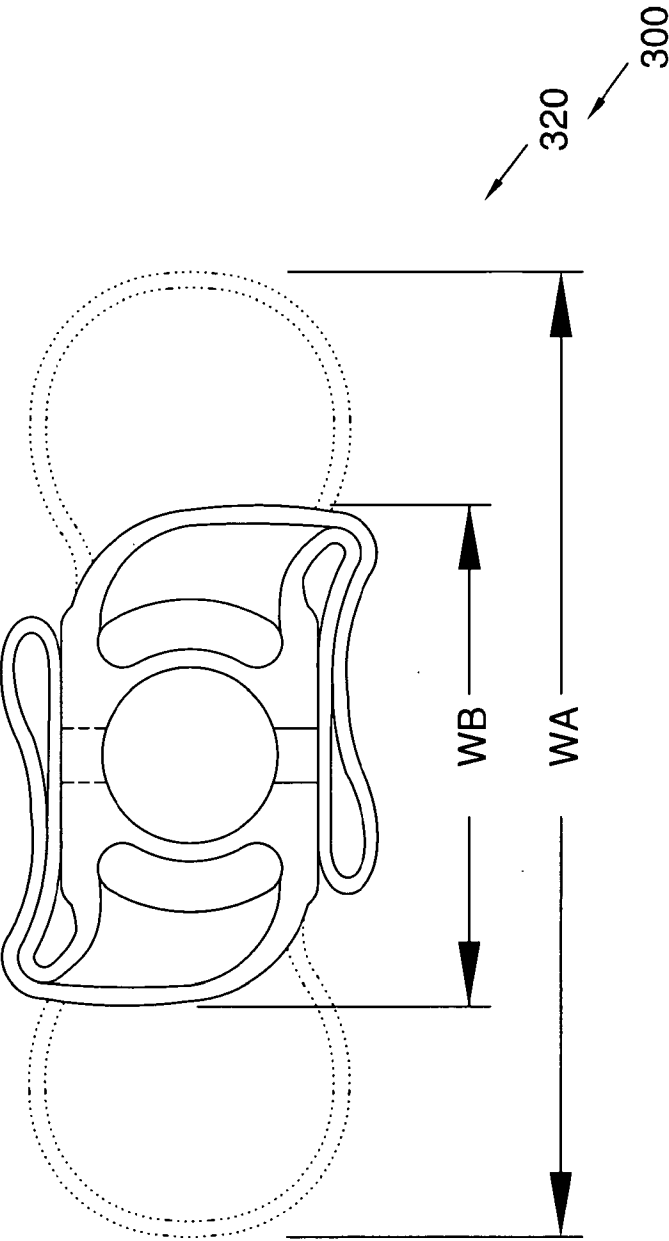


FIG. 20

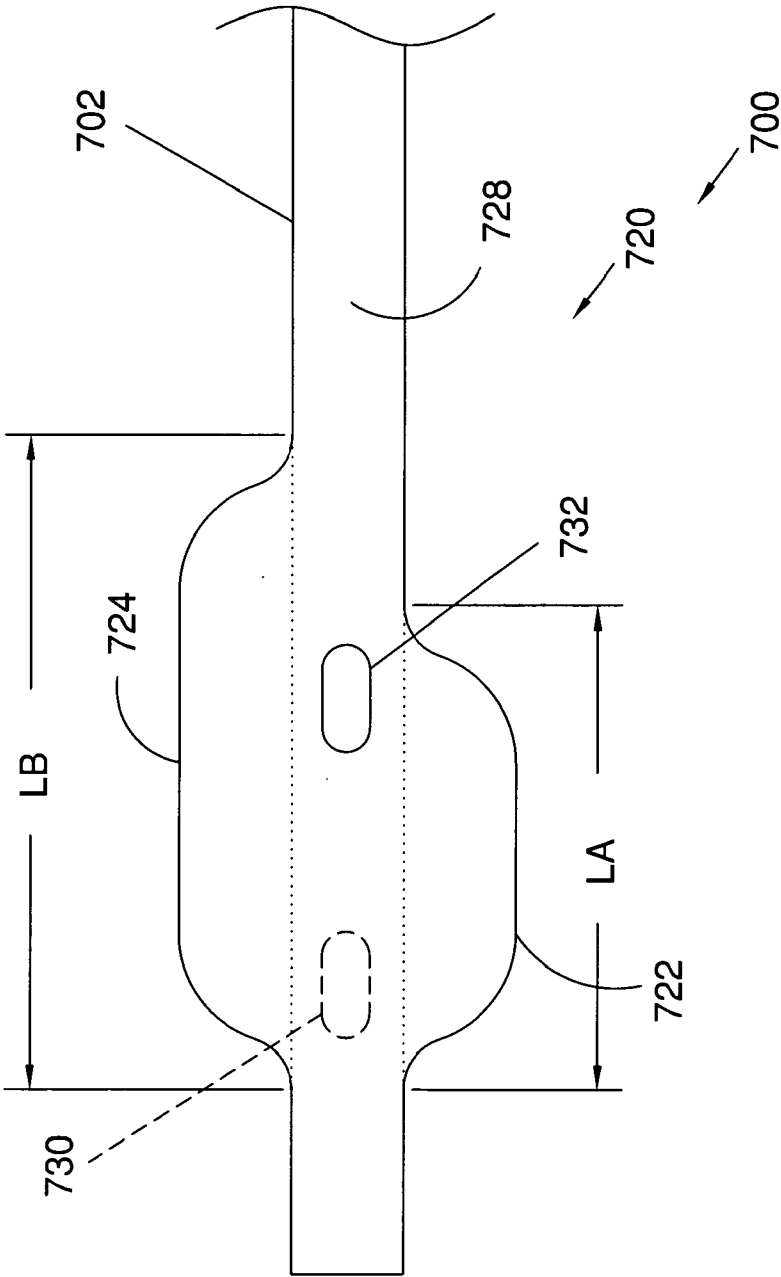


FIG. 21

INTERNATIONAL SEARCH REPORT

International application No
PCT/US2009/004634

A. CLASSIFICATION OF SUBJECT MATTER

INV. A61B17/3207 A61B17/221
ADD. A61B17/00 A61B17/22 A61B19/00 A61M25/10

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 2008/063621 A (BRIDGEPOINT MEDICAL INC [US]; KUGLER CHAD JOHN [US]; OLSON MATTHEW JON) 29 May 2008 (2008-05-29) figures 41-48	1-3, 6-12, 14-21
X	US 2007/265596 A1 (JEN JIMMY [US] ET AL) 15 November 2007 (2007-11-15) figure 7	1,6,7
E,L	WO 2009/100129 A (KUGLER CHAD JOHN [US]; OLSON MATTHEW JONATHAN [US]; OLSON ROSS ARLEN []) 13 August 2009 (2009-08-13) throws doubt on priority claim of the application figures 23-28	1-27

☐ Further documents are listed in the continuation of Box C.

☒ See patent family annex.

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"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

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"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

Date of the actual completion of the international search

23 November 2009

Date of mailing of the international search report

18/01/2010

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Authorized officer

Schießl, Werner

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/US2009/004634

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 2008063621 A	29-05-2008	EP 2101655 A2	23-09-2009
US 2007265596 A1	15-11-2007	NONE	
WO 2009100129 A	13-08-2009	US 2009209910 A1	20-08-2009