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Yao et al.

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(54) **MULTISPECTRAL SYNCHRONIZED IMAGING**

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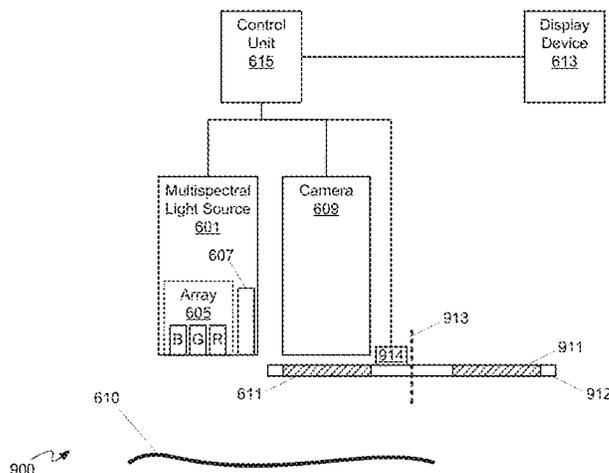
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(57) **ABSTRACT**

A multispectral synchronized imaging system is provided. A multispectral light source of the system includes: blue, green and red LEDs, and one or more non-visible light sources, each being independently addressable and configured to emit, in a sequence: at least visible white light, and non-visible light in one or more given non-visible frequency ranges. The system further includes a camera and an optical filter arranged to filter light received at the camera, by: transmitting visible light from the LEDs; filter out non-visible light from the non-visible light sources; and otherwise transmit excited light emitted by a tissue sample excited by non-visible light. Images acquired by the camera

(Continued)



are output to a display device. A control unit synchronizes acquisition of respective images at the camera for each of blue light, green light, visible white light, and excited light received at the camera, as reflected by the tissue sample.

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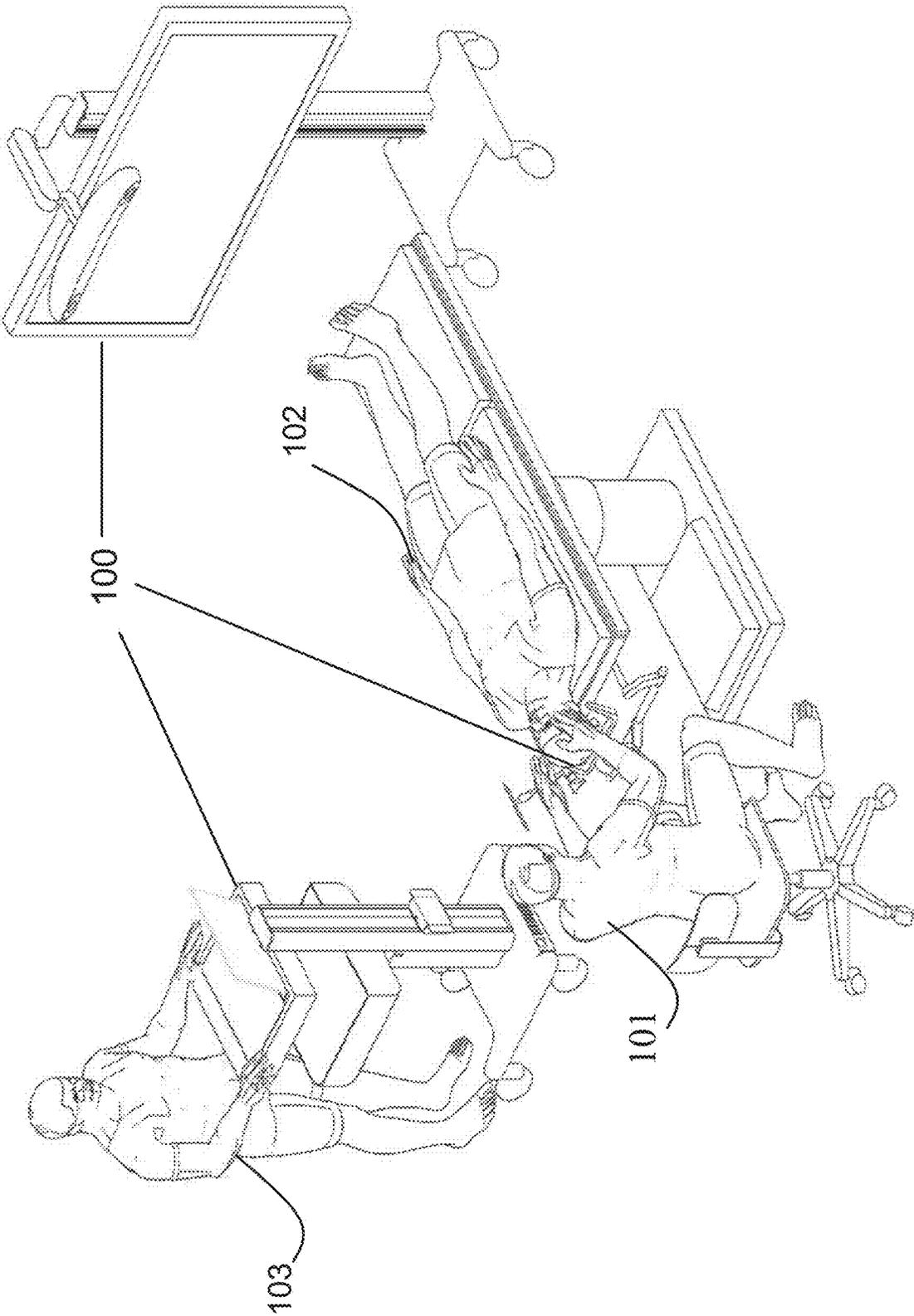


Figure 1

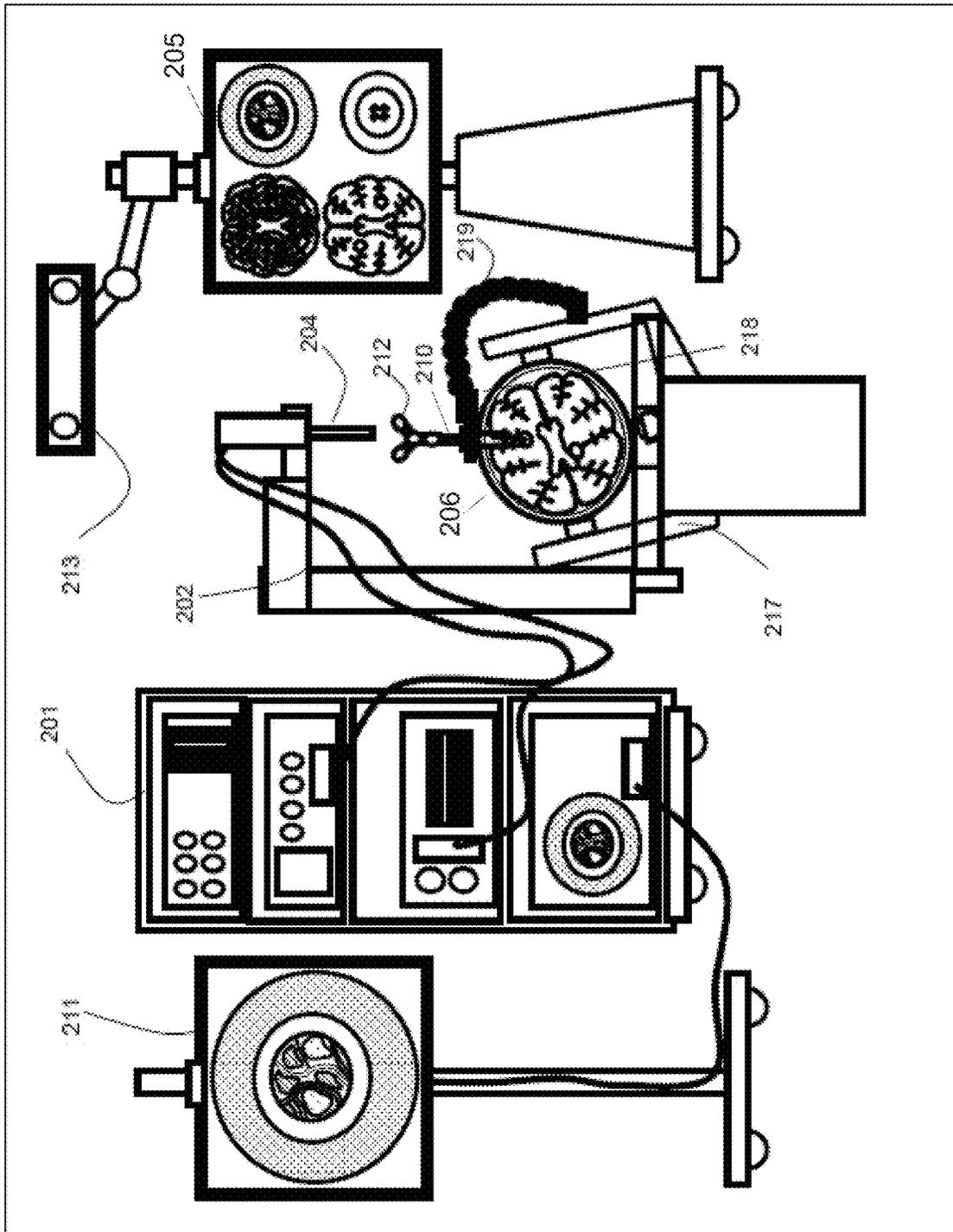


Figure 2

200

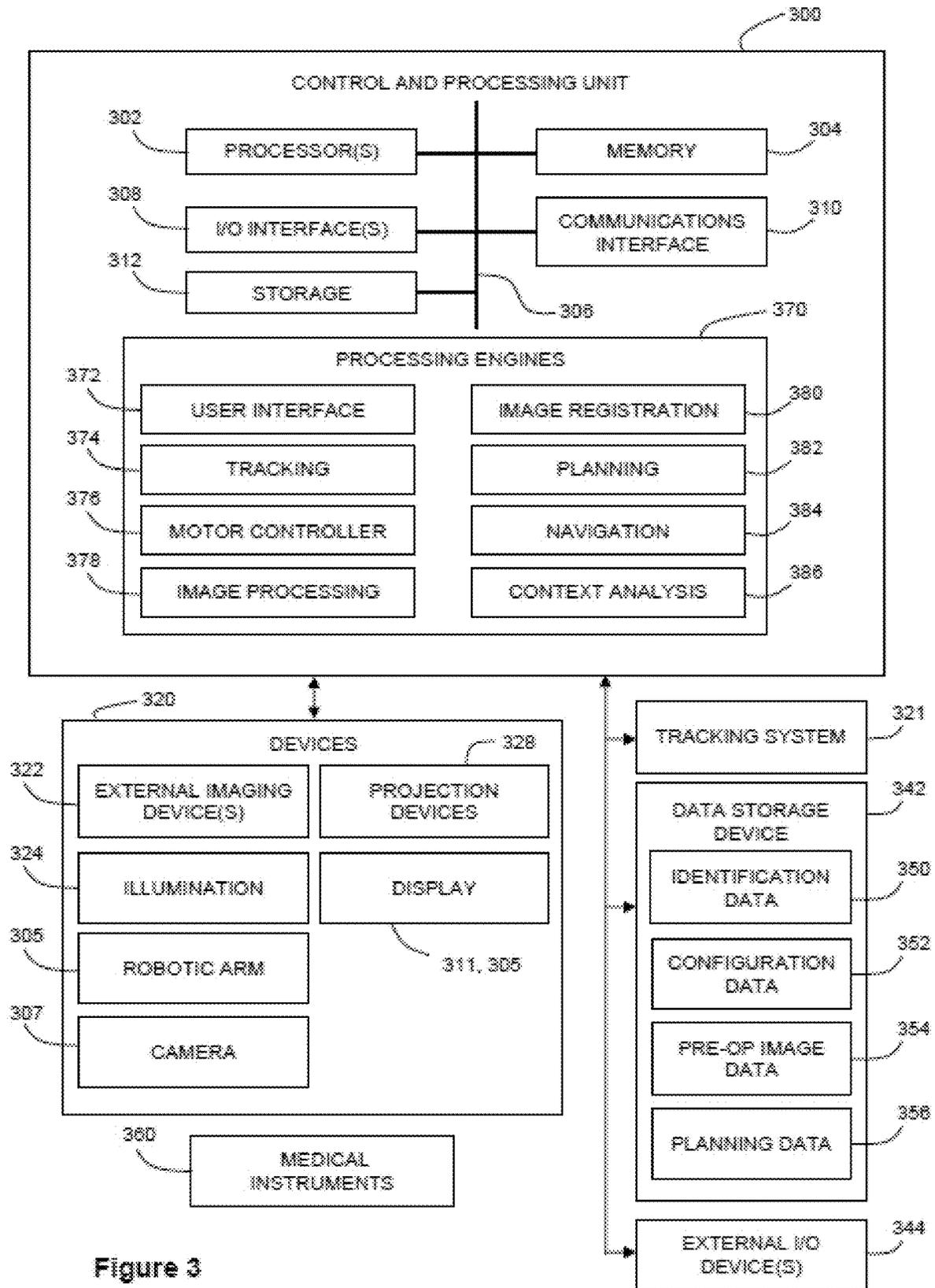


Figure 3

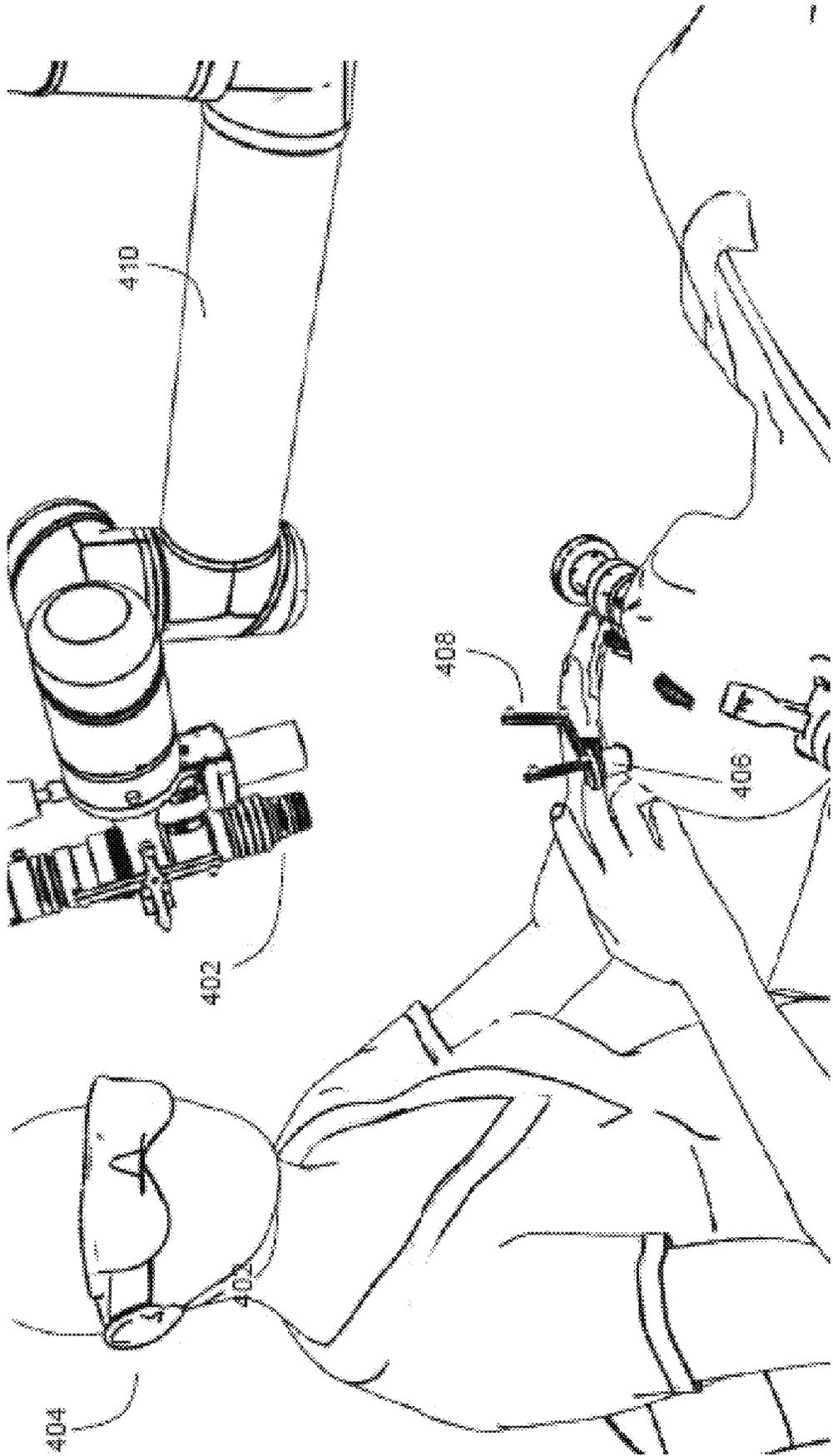


Figure 4

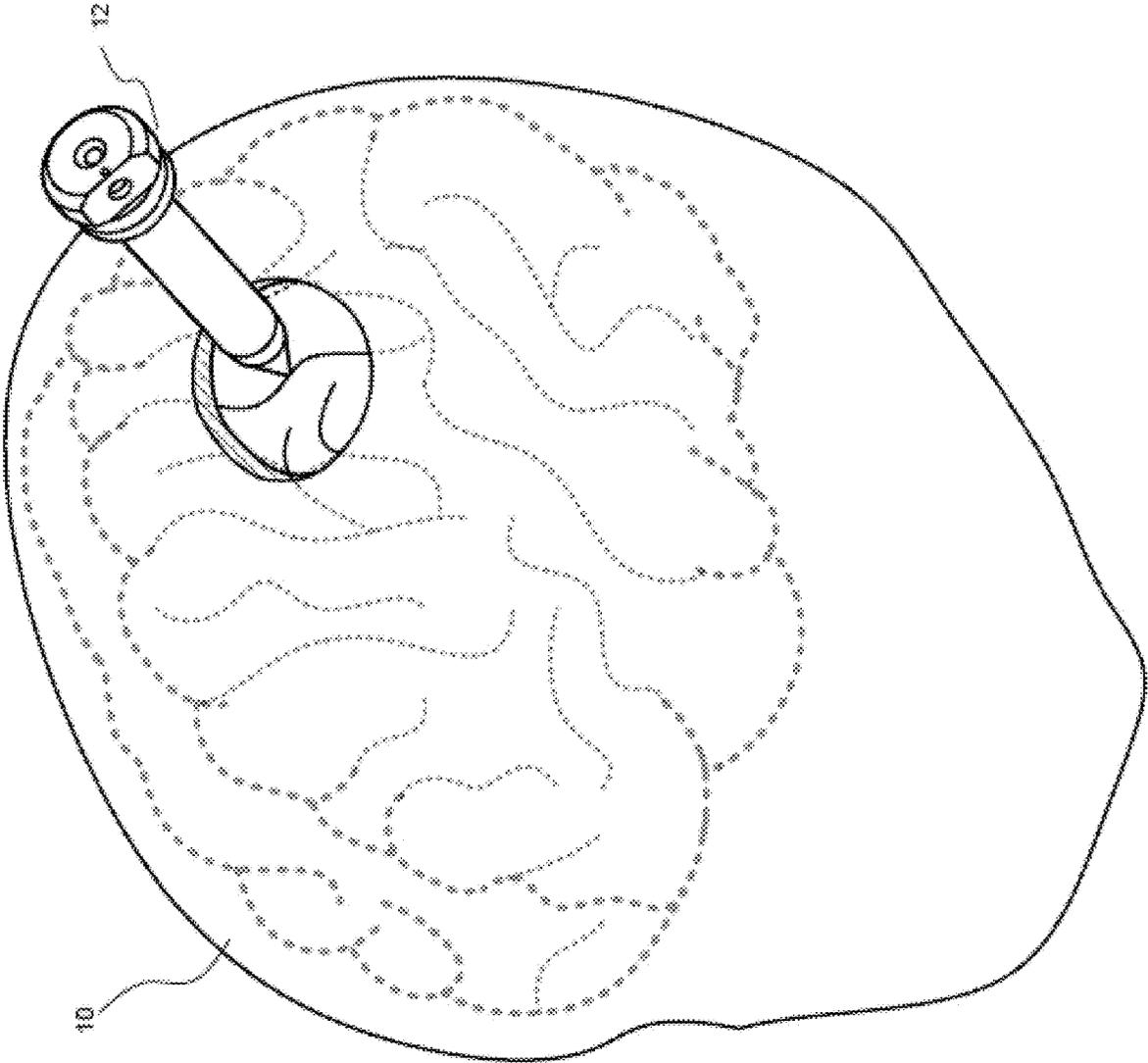


Figure 5

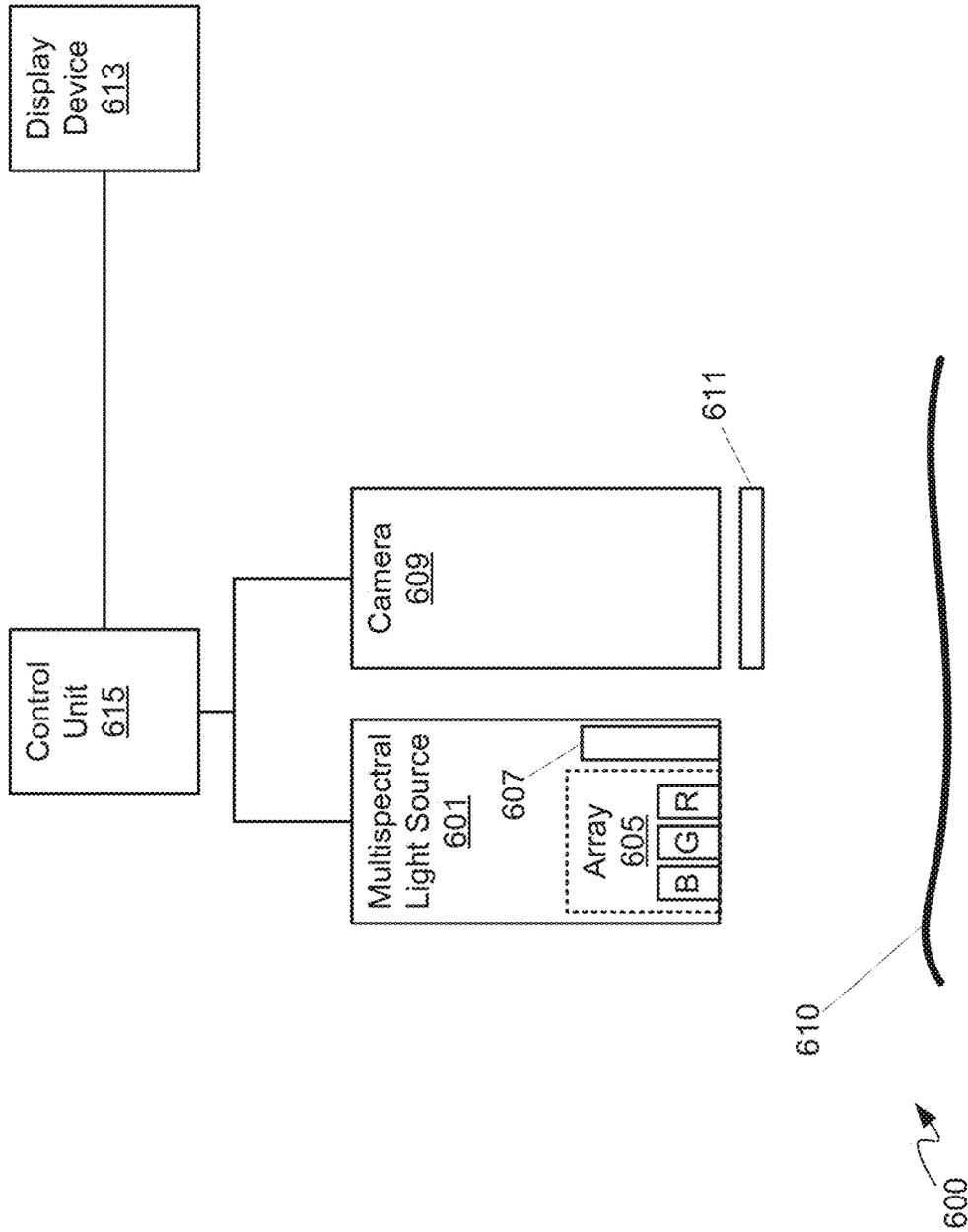


Figure 6

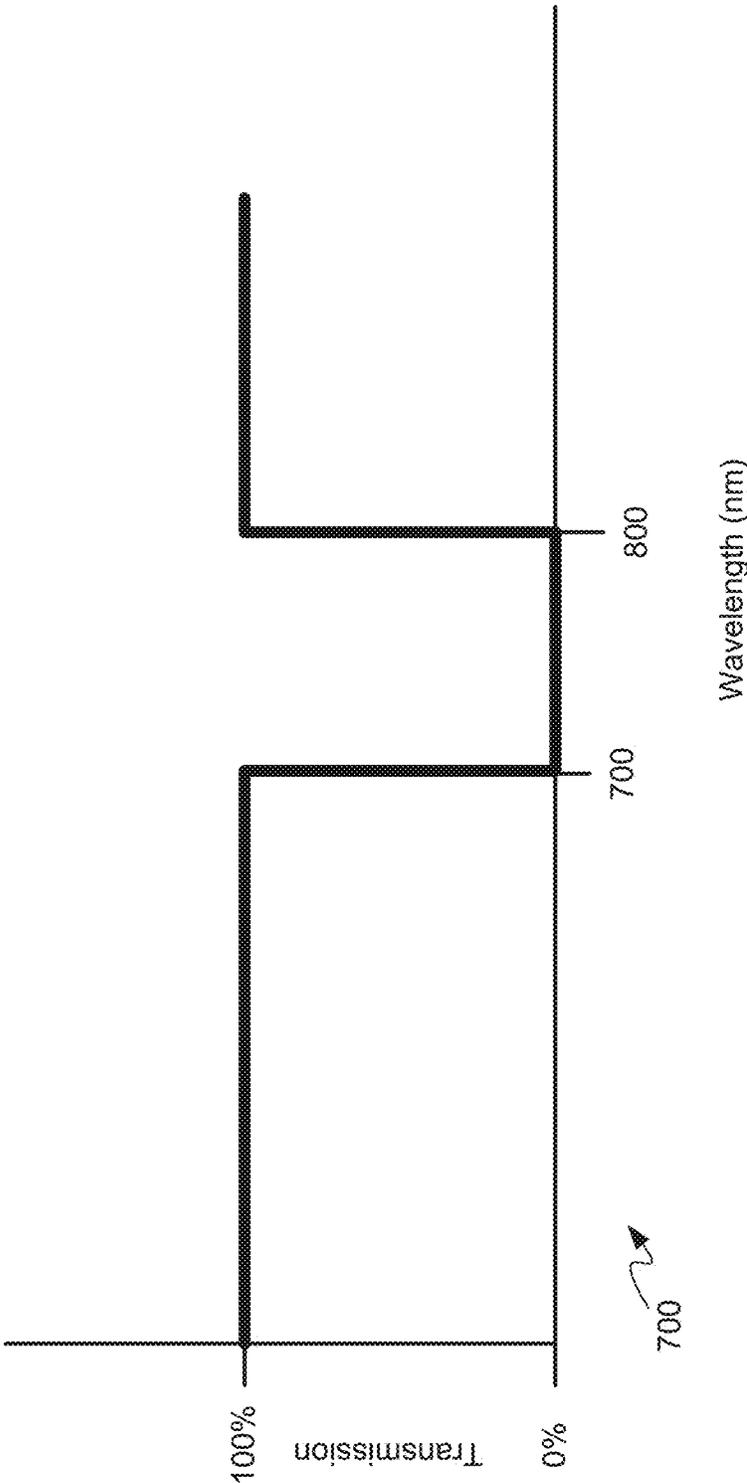


Figure 7

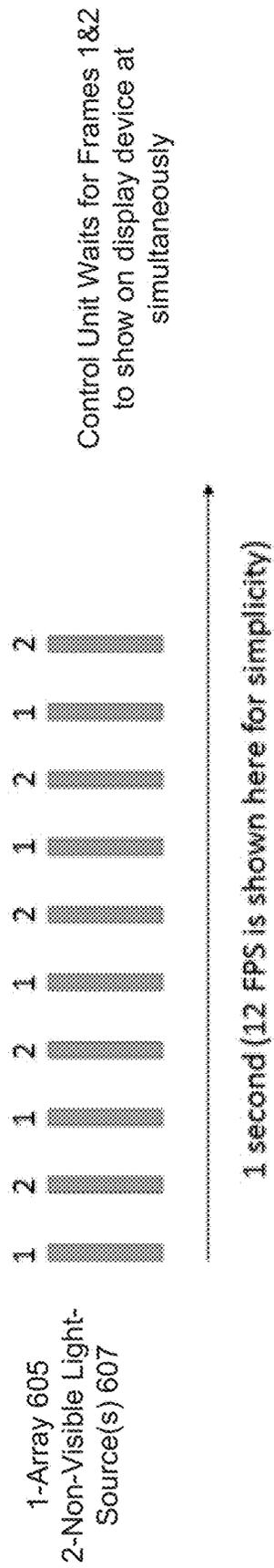


Figure 8

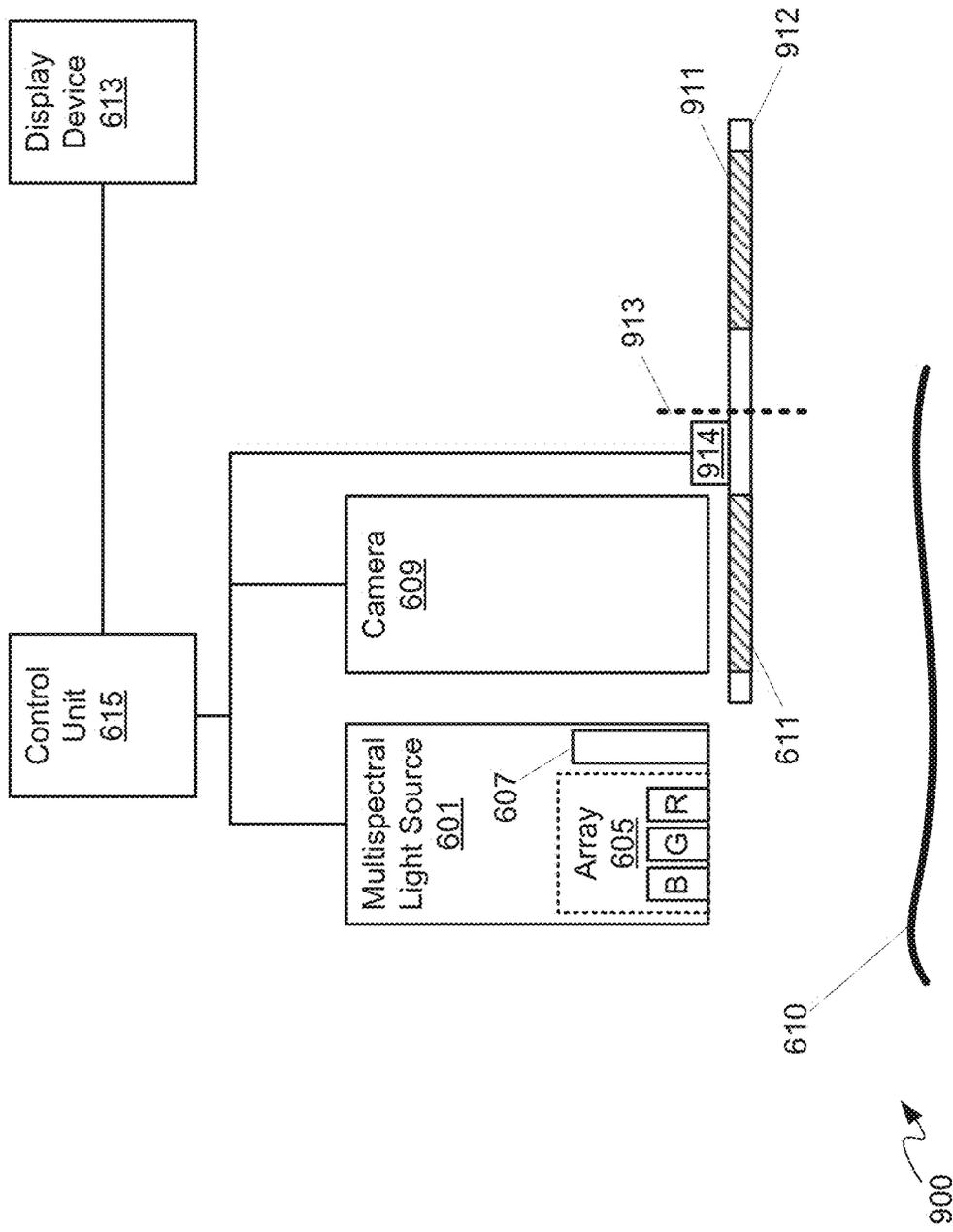


Figure 9

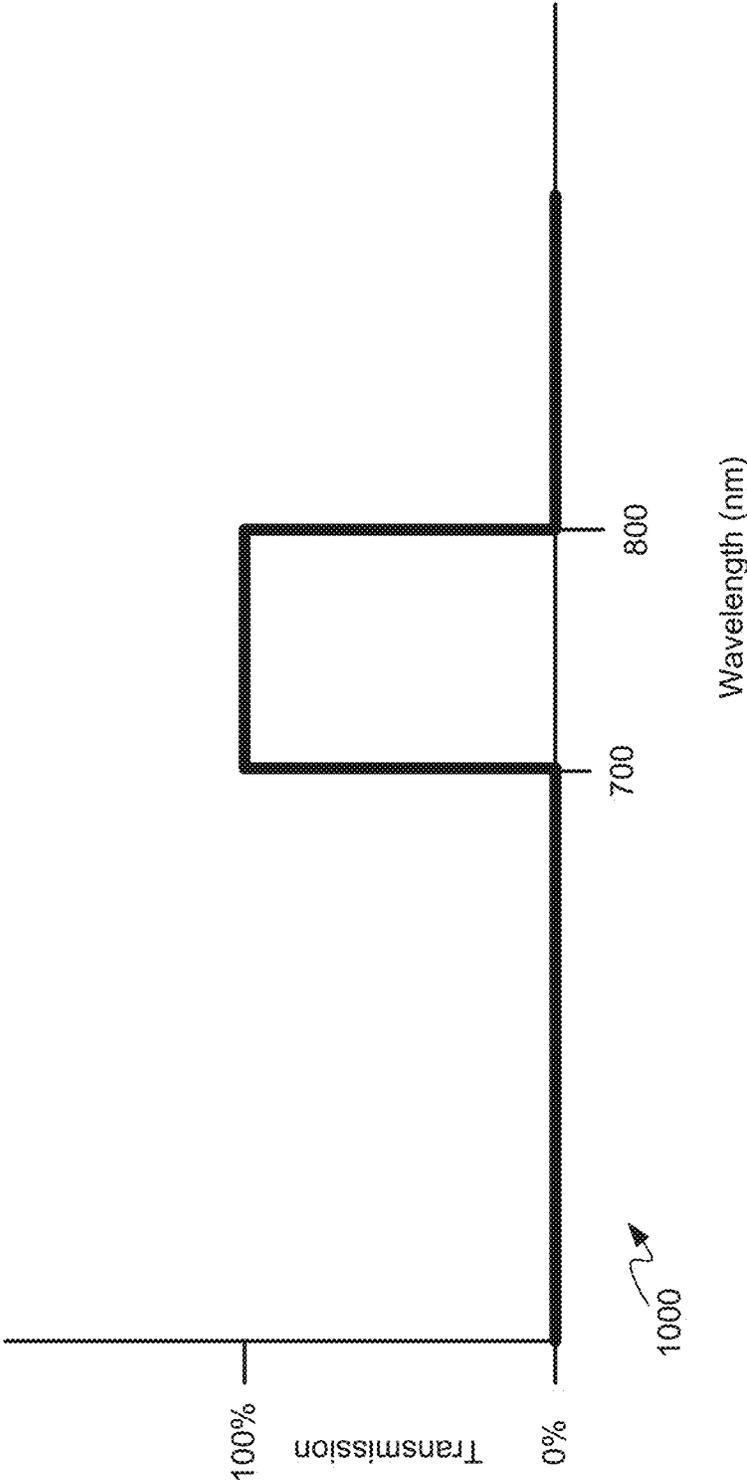


Figure 10

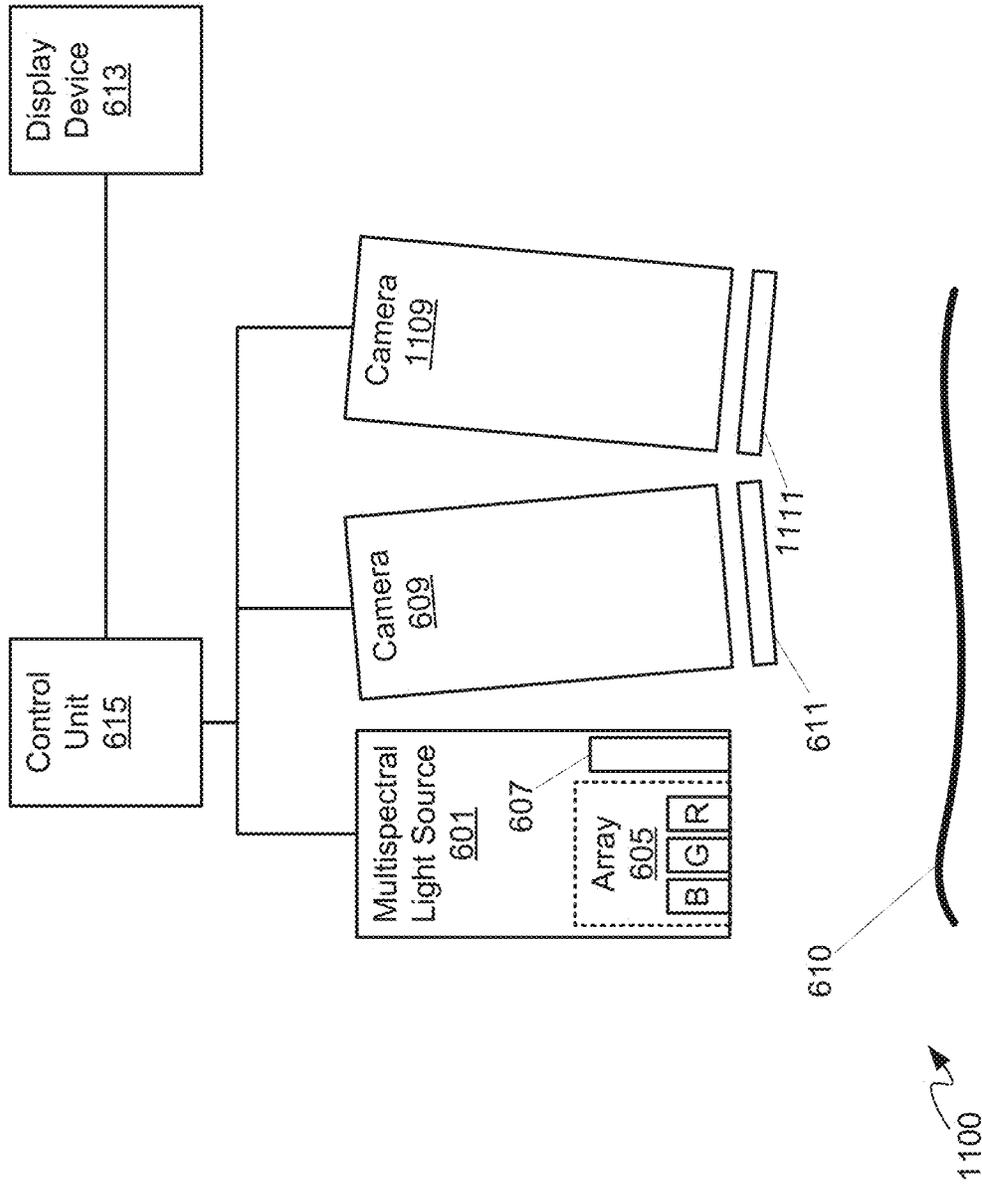


Figure 11

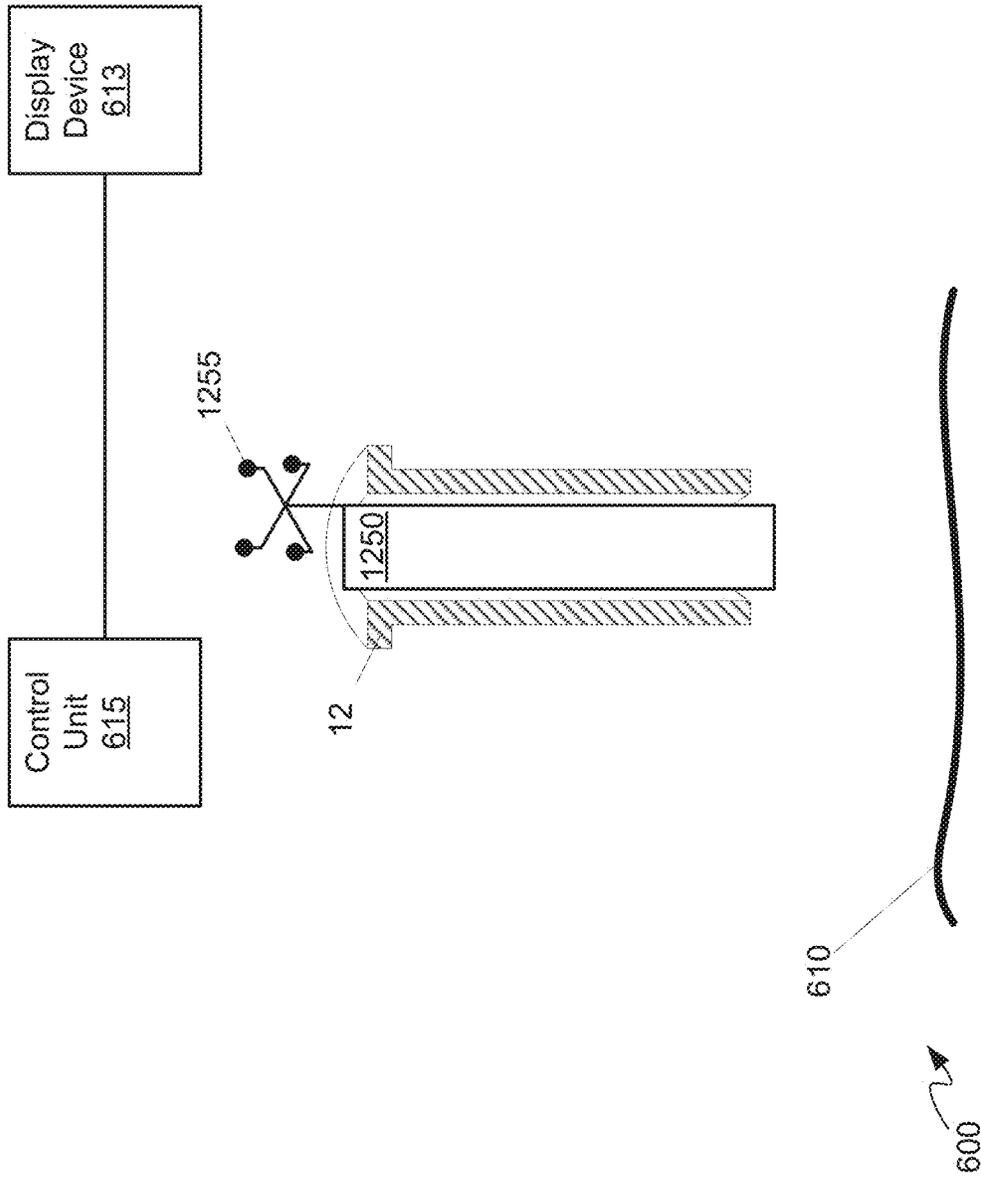


Figure 12

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**MULTISPECTRAL SYNCHRONIZED
IMAGING****CROSS-REFERENCE TO RELATED
APPLICATION(S)**

This document is a national phase entry application which claims the benefit of, and priority to, International Patent Application No. PCT/IB2016/052678, filed on May 10, 2016, entitled "MULTISPECTRAL SYNCHRONIZED IMAGING," which herein is incorporated by reference in its entirety.

FIELD

The specification relates generally to medical imaging and methods for minimally invasive therapy and image guided medical procedures, and specifically to a system and method of multispectral synchronized imaging.

BACKGROUND

Image guided medical procedures can include fluorescence guided surgery (FGS), which is a medical imaging technique used to facilitate the delineation of the tumor margin during surgery or vascular angiography. With the current mainstream technology, changing from normal white light surgery (WLS) to FGS requires a mechanical filter wheel for switching of the emission filter on the camera side and another filter wheel on the illumination side to constrict the wavelength to an optimal narrow band. This mechanical switching creates a significant delay that restricts the possibility of concurrent imaging of WLS and FGS. In addition, Indocyanine green (ICG) fluorescent dye, used in FGS, has an emission spectrum (820 nm-860 nm) can overlap with infrared tracking pulses used in intermittent tracking of surgical tools, which can create an artifact on the acquired image, restricting a concurrent tracking mode and ICG-FGS during surgery.

SUMMARY

The present disclosure is generally directed to image guided medical procedures using an access port. This port-based surgery approach allows a surgeon, or robotic surgical system, to perform a surgical procedure involving tumor resection in which the residual tumor remaining after is minimized, while also minimizing the trauma to the intact white and grey matter of the brain. In such procedures, trauma may occur, for example, due to contact with the access port, stress to the brain matter, unintentional impact with surgical devices, and/or accidental resection of healthy tissue.

Hence, an aspect of the present specification provides a multispectral synchronized imaging system comprising: a multispectral light source comprising: a light emitting diode (LED) array comprising: at least one blue LED, at least one green LED and at least one red LED; and one or more non-visible light sources arranged side by side with the LED array, each of the at least one blue LED, the at least one green LED, the at least one red LED, and the one or more non-visible light sources being independently addressable such that the multispectral light source is configured to emit in a sequence: at least visible white light, and non-visible light in one or more given non-visible frequency ranges; a camera arranged to receive light from a tissue sample illuminated by the multispectral light source in the sequence;

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an optical filter arranged to filter the light from the tissue sample received at the camera, the optical filter configured to: transmit visible light from the LED array; filter out non-visible light from the one or more non-visible light sources in the one or more given non-visible frequency ranges; and otherwise transmit excited light emitted by the tissue sample under excitation by the non-visible light from the one or more non-visible light sources; a display device; and, at least one control unit configured to: control the multispectral light source to emit the sequence; synchronize acquisition of respective images at the camera for each of blue light, green light, the visible white light, and the excited light received at the camera, as reflected by the tissue sample; and, output the respective images in a respective sequence to the display device.

The one or more non-visible light sources can comprise an ultraviolet (UV) LED, and the optical filter can be configured to filter out UV light from the UV LED, and transmit the excited light emitted by the tissue sample under excitation from the UV LED.

The one or more non-visible light sources can comprise an ultraviolet (UV) light source and an infrared (IR) light source, and the optical filter can be configured to: transmits light in a fluorescent range of about 430 nm to about 700 nm, and from about 820 nm to about 860 nm to allow light from emission of one or more of PpIX and ICG at the tissue sample to be imaged by the camera; and block light from both the UV light source and the IR light source from entering the camera

The one or more non-visible light sources can comprise an infrared (IR) laser, and the optical filter can be configured to filter out IR light from the IR laser, and transmit the excited light emitted by the tissue sample under excitation from the IR laser.

The one or more non-visible light sources can comprise an infrared (IR) laser, and the system can further comprise a second optical filter, exchangeable for the optical filter under control by the at least one control unit; the second optical filter can be configured to transmit light from the IR laser. The IR laser can be operable in one of a diffused mode, when the optical filter is filtering light to the camera, and a speckled mode when the second optical filter is filtering light to the camera. The IR laser can be operable in a speckled mode when the second optical filter is filtering light to the camera, and the sequence can include green light emitted from the green LED, and blue light emitted from the blue LED, when the optical filter is filtering light to the camera, speckled laser light from the IR laser in the speckled mode, the green light and the blue light used for functional imaging of blood flow in the tissue sample.

The sequence can comprise the visible white light, and the non-visible light alternating.

The sequence can comprise the visible white light, green light, blue light, and the non-visible light alternating.

The sequence can comprise: one or more of a user-configured sequence; and simultaneous emission of light from two or more of the at least one blue LED, the at least one green LED, the at least one red LED.

Respective relative intensity of each of the at least one blue LED, the at least one green LED, the at least one red LED can be adjusted to change one or more of: color temperature of the visible white light; and color rendering of the respective images at the display device.

The multispectral synchronized imaging system can further comprise: a second camera arranged relative to the camera to acquire three-dimensional images of the tissue sample; and a second optical filter can be configured to:

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transmit visible light from the LED array and transmit non-visible light from the one or more non-visible light sources in the one or more given non-visible frequency ranges. The one or more non-visible light sources can comprise an IR laser operable in one of a diffused mode and a speckled mode. The camera and the second camera can be configured to capture images independent of one another. Image capture times of each the camera and the second camera can be off-set with respect to one another.

The at least one control unit can be further configured to output the respective images in the respective sequence to the display device at a rate where the respective images appear simultaneously rendered to a human vision system.

The camera can comprise an optical camera.

The multispectral synchronized imaging system can further comprise a thermal camera arranged to receive the light from the tissue sample illuminated by the multispectral light source in the sequence.

The at least one control unit can comprise one or more ports configured for communicate with one or more of: external computing devices; electronic surgical devices; trackers; and infrared trackers.

The camera and the optical filter can be configured for use with a surgical port configured for corridor based surgery.

BRIEF DESCRIPTIONS OF THE DRAWINGS

For a better understanding of the various implementations described herein and to show more clearly how they may be carried into effect, reference will now be made, by way of example only, to the accompanying drawings in which:

FIG. 1 shows an example operating room setup for a minimally invasive access port-based medical procedure, according to non-limiting implementations.

FIG. 2 is a block diagram illustrating components of a medical navigation system that may be used to implement a surgical plan for a minimally invasive surgical procedure, according to non-limiting implementations.

FIG. 3 depicts a block diagram illustrating components of a planning system used to plan a medical procedure that may then be implemented using the navigation system of FIG. 2, according to non-limiting implementations.

FIG. 4 depicts an example implementation port based brain surgery using a video scope, according to non-limiting implementations.

FIG. 5 depicts insertion of an access port into a human brain, for providing access to interior brain tissue during a medical procedure, according to non-limiting implementations.

FIG. 6 depicts a multispectral synchronized imaging system, according to non-limiting implementations.

FIG. 7 depicts an example transmission spectrum of an optical filter in the multispectral synchronized imaging system of FIG. 6, according to non-limiting implementations.

FIG. 8 depicts a light emission sequence of a multispectral light source of the multispectral synchronized imaging system of FIG. 6, according to non-limiting implementations.

FIG. 9 depicts a multispectral synchronized imaging system adapted for use with multiple optical filters, according to non-limiting implementations.

FIG. 10 depicts an example transmission spectrum of one of the optical filters in the multispectral synchronized imaging system of FIG. 9, according to non-limiting implementations.

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FIG. 11 depicts a multispectral synchronized imaging system adapted for use with two cameras, according to non-limiting implementations.

FIG. 12 depicts a multispectral synchronized imaging system adapted for use with an access port for corridor based surgery, according to non-limiting implementations.

DETAILED DESCRIPTION

Various implementations and aspects of the specification will be described with reference to details discussed below. The following description and drawings are illustrative of the specification and are not to be construed as limiting the specification. Numerous specific details are described to provide a thorough understanding of various implementations of the present specification. However, in certain instances, well-known or conventional details are not described in order to provide a concise discussion of implementations of the present specification.

The systems and methods described herein may be useful in the field of neurosurgery, including oncological care, neurodegenerative disease, stroke, brain trauma and orthopedic surgery; however persons of skill will appreciate the ability to extend these concepts to other conditions or fields of medicine. It should be noted that the surgical process is applicable to surgical procedures for brain, spine, knee and any other suitable region of the body.

Various apparatuses and processes will be described below to provide examples of implementations of the system disclosed herein. No implementation described below limits any claimed implementation and any claimed implementations may cover processes or apparatuses that differ from those described below. The claimed implementations are not limited to apparatuses or processes having all of the features of any one apparatus or process described below or to features common to multiple or all of the apparatuses or processes described below. It is possible that an apparatus or process described below is not an implementation of any claimed subject matter.

Furthermore, numerous specific details are set forth in order to provide a thorough understanding of the implementations described herein. However, it will be understood by those skilled in the relevant arts that the implementations described herein may be practiced without these specific details. In other instances, well-known methods, procedures and components have not been described in detail so as not to obscure the implementations described herein.

In this specification, elements may be described as “configured to” perform one or more functions or “configured for” such functions. In general, an element that is configured to perform or configured for performing a function is enabled to perform the function, or is suitable for performing the function, or is adapted to perform the function, or is operable to perform the function, or is otherwise capable of performing the function.

It is understood that for the purpose of this specification, language of “at least one of X, Y, and Z” and “one or more of X, Y and Z” may be construed as X only, Y only, Z only, or any combination of two or more items X, Y, and Z (e.g., XYZ, XY, YZ, ZZ, and the like). Similar logic may be applied for two or more items in any occurrence of “at least one . . .” and “one or more . . .” language.

Referring to FIG. 1, a non-limiting example navigation system 100 is shown to support minimally invasive access port-based surgery. In FIG. 1, a neurosurgeon 101 conducts a minimally invasive port-based surgery on a patient 102 in an operating room (OR) environment. The navigation sys-

tem **100** includes an equipment tower, tracking system, displays and tracked instruments to assist the surgeon **101** during the procedure. An operator **103** may also be present to operate, control and provide assistance for the navigation system **100**.

Referring to FIG. 2, a block diagram is shown illustrating components of an example medical navigation system **200**, according to non-limiting implementations. The medical navigation system **200** illustrates a context in which a surgical plan including equipment (e.g., tool and material) tracking, such as that described herein, may be implemented. The medical navigation system **200** includes, but is not limited to, one or more monitors **205**, **211** for displaying a video image, an equipment tower **201**, and a mechanical arm **202**, which supports an optical scope **204**. The equipment tower **201** may be mounted on a frame (e.g., a rack or cart) and may contain a computer or controller (examples provided with reference to FIGS. 3 and 6 below), planning software, navigation software, a power supply and software to manage the mechanical arm **202**, and tracked instruments. In one example non-limiting implementation, the equipment tower **201** may comprise a single tower configuration with dual display monitors **211**, **205**, however other configurations may also exist (e.g., dual tower, single display, etc.). Furthermore, the equipment tower **201** may also be configured with a universal power supply (UPS) to provide for emergency power, in addition to a regular AC adapter power supply.

A patient's anatomy may be held in place by a holder. For example, in a neurosurgical procedure the patient's head may be held in place by a head holder **217**, and an access port **206** and an introducer **210** may be inserted into the patient's head. The introducer **210** may be tracked using a tracking camera **213**, which provides position information for the navigation system **200**. The tracking camera **213** may also be used to track tools and/or materials used in the surgery, as described in more detail below. In one example non-limiting implementation, the tracking camera **213** may comprise a 3D (three-dimensional) optical tracking stereo camera, similar to one made by Northern Digital Imaging (NDI), configured to locate reflective sphere tracking markers **212** in 3D space. In another example, the tracking camera **213** may comprise a magnetic camera, such as a field transmitter, where receiver coils are used to locate objects in 3D space, as is also known in the art. Location data of the mechanical arm **202** and access port **206** may be determined by the tracking camera **213** by detection of tracking markers **212** placed on these tools, for example the introducer **210** and associated pointing tools. Tracking markers may also be placed on surgical tools or materials to be tracked. The secondary display **205** may provide output of the tracking camera **213**. In one example non-limiting implementation, the output may be shown in axial, sagittal and coronal views as part of a multi-view display.

As noted above with reference to FIG. 2, the introducer **210** may include tracking markers **212** for tracking. The tracking markers **212** may comprise reflective spheres in the case of an optical tracking system and/or pick-up coils in the case of an electromagnetic tracking system. The tracking markers **212** may be detected by the tracking camera **213** and their respective positions are inferred by the tracking software.

As shown in FIG. 2, a guide clamp **218** (or more generally a guide) for holding the access port **206** may be provided. The guide clamp **218** may optionally engage and disengage with the access port **206** without needing to remove the access port **206** from the patient. In some examples, the

access port **206** may be moveable relative to the guide clamp **218**, while in the guide clamp **218**. For example, the access port **206** may be able to slide up and down (e.g., along the longitudinal axis of the access port **206**) relative to the guide clamp **218** while the guide clamp **218** is in a closed position. A locking mechanism may be attached to or integrated with the guide clamp **218**, and may optionally be actuatable with one hand, as described further below. Furthermore, an articulated arm **219** may be provided to hold the guide clamp **218**. The articulated arm **219** may have up to six degrees of freedom to position the guide clamp **218**. The articulated arm **219** may be lockable to fix its position and orientation, once a desired position is achieved. The articulated arm **219** may be attached or attachable to a point based on the patient head holder **217**, or another suitable point (e.g., on another patient support, such as on the surgical bed), to ensure that when locked in place, the guide clamp **218** does not move relative to the patient's head.

Referring to FIG. 3, a block diagram is shown illustrating a control and processing unit **300** that may be used in the navigation system **200** of FIG. 2 (e.g., as part of the equipment tower). In one example non-limiting implementation, control and processing unit **300** may include one or more processors **302**, a memory **304**, a system bus **306**, one or more input/output interfaces **308**, a communications interface **310**, and storage device **312**. In particular, one or more processors **302** may comprise one or more hardware processors and/or one or more microprocessors. Control and processing unit **300** may be interfaced with other external devices, such as tracking system **321**, data storage device **342**, and external user input and output devices **344**, which may include, but is not limited to, one or more of a display, keyboard, mouse, foot pedal, and microphone and speaker. Data storage device **342** may comprise any suitable data storage device, including, but not limited to a local and/or remote computing device (e.g. a computer, hard drive, digital media device, and/or server) having a database stored thereon. In the example shown in FIG. 3, data storage device **342** includes, but is not limited to, identification data **350** for identifying one or more medical instruments **360** and configuration data **352** that associates customized configuration parameters with one or more medical instruments **360**. Data storage device **342** may also include, but is not limited to, preoperative image data **354** and/or medical procedure planning data **356**. Although data storage device **342** is shown as a single device in FIG. 3, in other implementations, data storage device **342** may be provided as multiple storage devices.

Medical instruments **360** may be identifiable using control and processing unit **300**. Medical instruments **360** may be connected to and controlled by control and processing unit **300**, and/or medical instruments **360** may be operated and/or otherwise employed independent of control and processing unit **300**. Tracking system **321** may be employed to track one or more of medical instruments **360** and spatially register the one or more tracked medical instruments **360** to an intraoperative reference frame. In another example, a sheath may be placed over a medical instrument **360** and the sheath may be connected to and controlled by control and processing unit **300**.

Control and processing unit **300** may also interface with a number of configurable devices, and may intraoperatively reconfigure one or more of such devices based on configuration parameters obtained from configuration data **352**. Examples of devices **320**, as shown in FIG. 3, include, but are not limited, one or more external imaging devices **322**,

one or more illumination devices **324**, a robotic arm, one or more projection devices **328**, and one or more displays **305**, **311**.

Aspects of the specification may be implemented via processor(s) **302** and/or memory **304**. For example, the functionalities described herein may be partially implemented via hardware logic in processor **302** and partially using the instructions stored in memory **304**, as one or more processing modules **370** and/or processing engines. Example processing modules include, but are not limited to, user interface engine **372**, tracking module **374**, motor controller **376**, image processing engine **378**, image registration engine **380**, procedure planning engine **382**, navigation engine **384**, and context analysis module **386**. While the example processing modules are shown separately in FIG. **3**, in one example non-limiting implementation the processing modules **370** may be stored in the memory **304** and the processing modules may be collectively referred to as processing modules **370**.

It is to be understood that the system is not intended to be limited to the components shown in FIG. **3**. One or more components of the control and processing unit **300** may be provided as an external component or device. In one example non-limiting implementation, navigation engine **384** may be provided as an external navigation system that is integrated with control and processing unit **300**.

Some implementations may be implemented using processor **302** without additional instructions stored in memory **304**. Some implementations may be implemented using the instructions stored in memory **304** for execution by one or more general purpose microprocessors. Thus, the specification is not limited to a specific configuration of hardware and/or software.

While some implementations may be implemented in fully functioning computers and computer systems, various implementations are capable of being distributed as a computing product in a variety of forms and are capable of being applied regardless of the particular type of machine or computer readable media used to actually effect the distribution.

At least some aspects disclosed may be embodied, at least in part, in software. That is, the techniques may be carried out in a computer system or other data processing system in response to its processor, such as a microprocessor, executing sequences of instructions contained in a memory, such as ROM, volatile RAM, non-volatile memory, cache and/or a remote storage device.

A computer readable storage medium, and/or a non-transitory computer readable storage medium, may be used to store software and data which, when executed by a data processing system, causes the system to perform various methods. The executable software and data may be stored in various places including for example ROM, volatile RAM, non-volatile memory and/or cache. Portions of this software and/or data may be stored in any one of these storage devices.

Examples of computer-readable storage media include, but are not limited to, recordable and non-recordable type media such as volatile and non-volatile memory devices, read only memory (ROM), random access memory (RAM), flash memory devices, floppy and other removable disks, magnetic disk storage media, optical storage media (e.g., compact discs (CDs), digital versatile disks (DVDs), etc.), among others. The instructions may be embodied in digital and analog communication links for electrical, optical, acoustical and/or other forms of propagated signals, such as carrier waves, infrared signals, digital signals, and the like.

The storage medium may comprise the internet cloud, storage media therein, and/or a computer readable storage medium and/or a non-transitory computer readable storage medium, including, but not limited to, a disc.

At least some of the methods described herein are capable of being distributed in a computer program product comprising a computer readable medium that bears computer usable instructions for execution by one or more processors, to perform aspects of the methods described. The medium may be provided in various forms such as, but not limited to, one or more diskettes, compact disks, tapes, chips, USB (Universal Serial Bus) keys, external hard drives, wire-line transmissions, satellite transmissions, internet transmissions or downloads, magnetic and electronic storage media, digital and analog signals, and the like. The computer useable instructions may also be in various forms, including compiled and non-compiled code.

According to one aspect of the present application, one purpose of the navigation system **200**, which may include control and processing unit **300**, is to provide tools to a surgeon and/or a neurosurgeon that will lead to the most informed, least damaging neurosurgical operations. In addition to removal of brain tumors and intracranial hemorrhages (ICH), the navigation system **200** may also be applied to a brain biopsy, a functional/deep-brain stimulation, a catheter/shunt placement procedure, open craniotomies, endonasal/skull-based/ENT, spine procedures, and other parts of the body such as breast biopsies, liver biopsies, etc. While several examples have been provided, aspects of the present specification may be applied to other suitable medical procedures.

Attention is next directed to FIG. **4** which depicts a non-limiting example of a port-based brain surgery procedure using a video scope. In FIG. **4**, operator **404**, for example a surgeon, may align video scope **402** to peer down port **406**. Video scope **402** may be attached to an adjustable mechanical arm **410**. Port **406** may have a tracking tool **408** attached to it where tracking tool **408** is tracked by a tracking camera of a navigation system.

Even though the video scope **402** may comprise an endoscope and/or a microscope, these devices introduce optical and ergonomic limitations when the surgical procedure is conducted over a confined space and conducted over a prolonged period such as the case with minimally invasive brain surgery.

FIG. **5** illustrates the insertion of an access port **12** into a human brain **10**, in order to provide access to interior brain tissue during a medical procedure. In FIG. **5**, access port **12** is inserted into a human brain **10**, providing access to interior brain tissue. Access port **12** may include, but is not limited to, instruments such as catheters, surgical probes, and/or cylindrical ports such as the NICO BrainPath. Surgical tools and instruments may then be inserted within a lumen of the access port **12** in order to perform surgical, diagnostic or therapeutic procedures, such as resecting tumors as necessary. However, the present specification applies equally well to catheters, DBS needles, a biopsy procedure, and also to biopsies and/or catheters in other medical procedures performed on other parts of the body.

In the example of a port-based surgery, a straight and/or linear access port **12** is typically guided down a sulci path of the brain. Surgical instruments and/or surgical tools would then be inserted down the access port **12**.

Attention is next directed to FIG. **6**, which depicts an example of a multispectral medical imaging system **600** that could be used with access port **12**. System **600** comprises: a multispectral light source **601** comprising: a light emitting

diode (LED) array **605** comprising: at least one blue LED (as indicated by “B” in FIG. 6), at least one green LED (as indicated by “G” in FIG. 6) and at least one red LED (as indicated by “R” in FIG. 6); and one or more non-visible light sources **607** arranged side by side with LED array **605**, each of the at least one blue LED, the at least one green LED, the at least one red LED, and the one or more non-visible light sources **607** being independently addressable such that multispectral light source **601** is configured to emit in a sequence: at least visible white light, and non-visible light in one or more given non-visible frequency ranges; a camera **609** arranged to receive light from a tissue sample **610** illuminated by multispectral light source **601** in the sequence; an optical filter **611** arranged to filter the light from tissue sample **610** received at camera **609**, the optical filter configured to: transmit visible light from LED array **605**; filter out non-visible light from the one or more non-visible light sources **607** in the one or more given non-visible frequency ranges; and otherwise transmit excited light emitted by tissue sample **610** under excitation by the non-visible light from the one or more non-visible light sources **607**; a display device **613**; and, at least one control unit **615** configured to: control multispectral light source **601** to emit the sequence; synchronize acquisition of respective images at the camera **609** for each of blue light, green light, the white light, and the excited light received at camera **609**, as reflected by tissue sample **610**; and, output the respective images in a respective sequence to display device **613**.

For clarity, appreciated is that the terms visible and non-visible, as used herein, refer to a human vision system (HVS). Hence, the term “visible light,” as used herein, comprises light that is considered visible in a human vision system and/or is visible to an average human being. Similarly, the term “non-visible light,” as used herein, comprises light that is considered non-visible in a human vision system and/or is non-visible to an average human being.

While not depicted, multispectral light source **601**, camera **609** and optical filter **611** can be adapted for use with access port **12** and/or corridor based surgery and the like. In other words, spectral light source **601**, camera **609** and filter **611** can be components of an endoscope, and the like, used with access port **12** and/or corridor based surgery and the like. Put another way, multispectral light source **601**, camera **609** and optical filter **611** can be configured for use with a surgical port configured for corridor based surgery, as described in more detail below with respect to FIG. 12.

Components of system **600** will now be described in detail. In particular, multispectral light source **601**, which will interchangeably referred to hereafter as light source **601**, can comprise an integrated light source, for example, that includes LED array **605** (interchangeably referred to hereafter as array **605**) and one or more non-visible light sources **607**. While only one LED is depicted for each color LED in array **605** in FIG. 6, array **605** can include arrays of LEDs for each color. One or more non-visible light sources **607** can include, but is not limited, one or more infrared (IR) diodes and/or one or more IR lasers and/or one or more ultraviolet (UV) diodes and/or one or more UV laser.

Camera **609** can include, but is not limited to one or more of a CCD camera, a digital camera, an optical camera, and the like, and is generally configured to acquire digital images.

Optical filter **611**, which will be described in more detail below, can comprise a dichroic filter and the like, and can be located at least in front of an image sensor of camera **609**

and/or in front of a lens of camera **609**. Either way, light imaged by camera **609** is generally filtered by optical filter **611**.

As described above, optical filter **611** is configured to: transmit visible light from LED array **605**; filter out non-visible light from one or more non-visible light sources **607** in the one or more given non-visible frequency ranges; and otherwise transmit excited light emitted by tissue sample **610** under excitation by the non-visible light from the one or more non-visible light sources **607**; a display device **613**. In other words, optical filter transmits light from LEDs in array **605**, does not transmit light from one or more non-visible light sources **607**, but transmits light emitted from tissue sample **610** when excited by non-visible light from one or more non-visible light sources **607**.

As such, a transmission spectrum of optical filter **611** is selected for compatibility with one or more non-visible light sources **607**, and any specific imaging techniques and/or dyes to be used in tissue sample **610** during surgery. For example, tissue sample **610** can be treated with a given dye, including, but not limited to fluorescence dyes that fluoresce when irradiated by non-visible light (including, but not limited to one or more of PpIX fluorophore, that fluoresces when irradiated by UV light, and ICG fluorophore, that fluoresces when irradiated by IR light). As such, in this example, a transmission spectrum of optical filter **611** can be selected that transmits fluorescent light emitted by tissue sample **610**, but does not transmit and/or blocks the excitation light from one or more non-visible light sources **607**.

Hence, in some implementations, one or more non-visible light sources **607** comprises an ultraviolet (UV) LED, and the like, and optical filter **611** is configured to filter out UV light from the UV LED, and transmit the excited light emitted by tissue sample **610** under excitation from the UV LED.

Alternatively, in other implementations, one or more non-visible light sources **607** comprises an infrared (IR) laser, and the like, and optical filter **611** is configured to filter out IR light from the IR laser, and transmit the excited light emitted by tissue sample **610** under excitation from the IR laser.

However, in other implementations, one or more non-visible light sources **607** can comprise both a UV light source and an IR light source, and optical filter **611** can be adapted accordingly to block light from both.

Attention is directed to FIG. 7 which depicts a non-limiting transmission spectrum **700** of optical filter **611**, assuming that one or more non-visible light sources **607** comprises an infrared (IR) laser, and the like, and optical filter **611** is configured to filter out IR light from the IR laser, and transmit the excited light emitted by tissue sample **610** under excitation from the IR laser. Specifically, it is assumed in FIG. 7 that the IR laser emits light in a range of about 700 nm to about 800 nm and that tissue sample **610** emits light above about 800 nm when irradiated by light from the IR laser. Hence, in the range of about 700 nm to about 800 nm, light is not transmitted by optical filter **611** (e.g. transmission is about 0%), but outside of the range of about 700 nm to about 800 nm, light is transmitted (e.g. transmission is about 100%). Hence, in these implementations, camera **609** can image light in the visible range below 700 nm from LED array **605** that is reflected to camera **609** by tissue sample **610**, and camera **609** can also image light emitted by tissue sample **610** when excited by light from one or more non-visible light sources **607**.

While a specific range of wavelengths where the light is not transmitted is depicted in FIG. 7, in other implementa-

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tions, other ranges of wavelengths can be selected that are compatible with light emitted from one or more non-visible light sources 607. Furthermore, while not depicted, optical filter 611 can be further configured to block transmission of light below a visible range of wavelengths and/or in a UV range of wavelengths, and/or configured to block transmission of light above a given wavelength (e.g. above 900 nm, or 1000 nm and/or in the far infrared, to ensure that far IR light does not interfere with operation of system 600)

Returning to FIG. 6, display device 613 can comprise any suitable display device including, but not limited to, cathode ray tubes, flat panel displays, and the like. For example, display device 613 can comprise one or more of monitors 205, 211, as depicted in FIG. 2, and/or displays 305, 311 depicted in FIG. 3.

At least one control unit 615 is generally configured to control light source 601 and display device 613 and to receive images from camera 609. Hence, at least one control unit 615 is interconnected with each of light source 601, camera 609 and display device 613. In some implementations, at least one control unit 615 can comprise control and processing unit 300 depicted in FIG. 3, and/or at least one control unit 615 can be in communication with control and processing unit 300 depicted in FIG. 3 and/or at least one control unit 615 can be under control of communication with control and processing unit 300 depicted in FIG. 3.

At least one control unit 615 can further comprise any suitable combination of computing devices, processors, memory devices and the like. In particular, at least one control unit 615 can comprise one or more of a data acquisition unit, configured to acquire data and/or images at least from camera 609, and an image processing unit, configured to process data and/or images from camera 609 for rendering at display device 613.

In particular, at least one control unit 615 controls control multispectral light source 601 to emit light in a sequence that includes visible white light (e.g. from array 605) and non-visible light (e.g. from one or more non-visible light sources 607). Hence, at least one control unit 615 causes tissue sample 610 to be irradiated with at least white light and non-visible light in a sequence (e.g. see FIG. 8, described below). The sequence can also include blue light emitted from the blue LED, and green light emitted from the green LED.

Tissue sample 610 reflects the white light (and blue light and green light) into camera 609 through optical filter 611, and emits excited light under excitation from the non-visible light from one or more non-visible light sources 607, which is also received at camera 609 through optical filter 611 (which also removes the non-visible light from one or more non-visible light sources 607). Hence, camera 609 alternately (and/or in a sequence), produces optical images of tissue sample 610 when irradiated with white light, blue light and green light, and images of the excited light emitted by tissue sample 610.

Hence at least one control unit 615 is also configured to synchronize acquisition of respective images at camera 609 for each of the blue light, the green light, the white light, and the excited light received at camera 609, as reflected and/or emitted by tissue sample 610. For example, at least one control unit 615 can track when multispectral light source 601 is emitting a particular color and/or type of light (e.g. green, blue, white, non-visible), and can classify an image received from camera 609 simultaneous with such emission as being generated using the particular color and/or type of light. Hence, at least one control unit 615 can coordinate

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emission of light from multispectral light source 601 with acquisition of images produced by the light at camera 609.

Respective images that result from each particular color and/or type of light is output in a respective sequence to display device 613 for rendering thereupon. Such images can, for example, assist a surgeon with guiding surgical tools in an access port during corridor based surgery. For example, images produced using visible light can be used for an optical view of tissue sample 610, while images produced from excited light from tissue sample 610 can be used for fluorescence guided surgery; indeed, using system 600, a surgeon can switch back and forth between white light guided surgery (and/or surgery using blue light and/or green light) and fluorescence guided surgery.

Indeed, various sequence of light used to irradiate tissue sample 610 are within the scope of present implementations. For example, the sequence can comprise the visible white light, and the non-visible light alternating. Alternatively, the sequence can comprises visible white light, green light, blue light, and the non-visible light, alternating. However, the sequence can also comprise: one or more of a user-configured sequence; and simultaneous emission of light from two or more of the at least one blue LED, the at least one green LED, the at least one red LED. Indeed, any sequence that will assist a surgeon view tissue sample 610 using images rendered at display device 613 is within the scope of present implementations.

In some implementations, at least one control unit 615 can further control intensity of LEDs in array 605. For example, respective relative intensity of each of the at least one blue LED, the at least one green LED, the at least one red LED can be adjusted to change one or more of color temperature of the visible white light and color rendering of respective images output to display device 613. For example, color quality of light and/or white light can be described by two parameters: correlated color temperature (CCT) and color rendering index (CRI), and by respective relative intensity of each of the at least one blue LED, the at least one green LED, the at least one red LED, a given and/or desired CCT and CRI can be provided to, in turn, achieve a given color appearance of tissue sample 610, including a CCT and CRI within desired ranges (e.g. for a "good" color appearance).

In any event, attention is next directed to FIG. 8, which depicts a sample sequence that can be implemented at multispectral light source 601 in which light from array ("1") 605 alternates with non-visible light ("2") from one or more non-visible light sources 607. In particular, the sequence depicted in FIG. 8 comprise the visible white light, and the non-visible light alternating, at a rate of 12 frames per second (FPS), which is also the rate at which the corresponding images are rendered at display device 613.

Indeed, images rendered at display device 613 can be at a rate (with multispectral light source 601 controlled at a corresponding rate) where the images appear to be simultaneously rendered to a human vision system. Hence, for example, images that result from tissue sample 610 being irradiated with white light appear to be combined with images formed from excited light emitted from tissue sample 610, thereby combining white light surgery and fluorescence guided surgery, and the like; in other words, features of tissue sample 610 that are visible only using fluorescence guided surgery are combined at display device 613 with features of tissue sample 610 visible when tissue sample 610 is irradiated with white light.

Hence, at least one control unit 615 can be further configured to output the respective images in the respective sequence to display device 613. In some implementations,

such images can be static, for example, one or more acquired images can be rendered at display device 613, statically (e.g. one or more images are acquired and rendered at display device 613 rather than a stream of images). In other implementations, least one control unit 615 can be further configured to output the respective images in the respective sequence to display device 613 in a video stream and/or at a rate where the respective images appear simultaneously rendered to a human vision system. For example, in some implementations, such rates can, include, but are not limited to, 12 FPS and higher. However, the rate of rendering images at display device 613 can also depend on a rate at which images are acquired at camera 609; for example, if camera acquires images at a rate of 60 Hz, an output rate of images at display device 613 can be about half the camera rate and/or about 30 Hz, assuming that two frames are captured, one visible and one-non-visible (e.g. see FIG. 8, described below). However, other rates are within the scope of present implementations and can depend both on a configuration of camera 609 and/or a configuration of display device 613 and/or a number of light sources in multispectral light source 601 and/or a number of frames dedicated to each of the light sources in multispectral light source 601.

Indeed, LEDs of array 605, as well as one or more non-visible light sources 607 can be selected based on what rate images are to be provided at display device 613. For example, specific LEDs types (for array 605) and laser diodes (for one or more non-visible light sources 607) can be selected where transient times are less than a microsecond.

Similarly, wavelengths of each of LEDs of array 605 and laser diodes for one or more non-visible light sources 607 can be selected which maximize a number of modalities that can be measured in conjunction with the camera synchronization. In a particular non-limiting implementation, two types of laser diodes can be used at one or more non-visible light sources 607 that emit both UV light and IR light; in one particular non-limiting implementation, array 605 can comprise: one or more 460 nm Blue LEDs, one or more 530 nm Green LEDs; and one or more 620 nm Red LEDs, and non-visible light sources 607 can comprise: one or more 415 nm UV LEDs, and one or more 785 nm IR laser diodes. As such, a transmission spectrum of optical filter 611 is adapted to transmit light in the range if the LEDs of array 605, and to block light emitted by both the one or more 415 nm UV LEDs, and the one or more 785 nm IR laser diodes.

Use of such LEDs, UV LEDs and IR laser diodes can enable several modes and/or use cases in system 600 which can include, but is not limited to:

UV LED: excitation of PpIX fluorophore for better tumor margin delineation (e.g. to produce excited light from a tissue sample);

Blue/Green/Red LEDs: trichromatic white light with tunable CRI (color rendering index);

Blue/Green interleaved: quantitative measure of blood oxygenation and volume (i.e. the sequence can include blue and green light);

Diffused IR laser: excitation of ICG fluorophore for angiography (e.g. to produce excited light from a tissue sample); and,

Speckled IR laser: quantitative measure of the blood flow.

In the last use case, system 600 can be modified to include at least a second optical filter that can be exchanged for optical filter 611, the second optical filter and optical filter 611 being exchangeable, depending on the operating mode.

For example, attention is next directed to FIG. 9 which depicts system 900 and is substantially similar to system 600, with like elements having like numbers, however in

system 900, one or more non-visible light sources 607 specifically comprises an infrared (IR) laser, and system 900 further comprising a second optical filter 911, that can be exchanged for optical filter 611 under control by at least one control unit 615, second optical filter 911 configured to transmit light from the IR laser.

For example, as depicted, optical filters 611, 911 can be mounted in a filter wheel 912 configured to rotate about an axis 913. In other words, in FIG. 9 depicts a cross-sectional view of filter wheel 912. Furthermore, filter wheel 912 further comprises apparatus 914 configured to control a position of optical filters 611, 911 with respect to camera 609, apparatus 914 in communication with at least one control unit 615. For example, apparatus 914 can comprise a stepper motor, and the like. Alternatively optical filters 611, 911 can be mounted to a slideable arm, and the like, configured to exchange optical filters 611, 911 under control by at least one control unit 615; indeed, any device for exchanging optical filters 611, 911 under control by at least one control unit 615 is within the scope of present implementations, assuming such devices are compatible with the surgical techniques to be used with system 900.

Attention is next directed to FIG. 10, which depicts a transmission spectrum 1000 of optical filter 911. In contrast to the transmission spectrum 700 of optical filter 611 depicted in FIG. 7, transmission spectrum 1000 of optical filter 911 transmits light from IR laser of one or more non-visible light sources 607 in a range of about 700 nm to about 800 nm, and does not transmit light outside this range.

Hence, optical filter 611 can be used to operate system 900 in a manner similar to system 600 and described above. However, optical filter 911 can be exchanged for optical filter 611, and the IR laser of one or more non-visible light sources 607 can be operated in a speckled mode which can be used to quantitatively measure blood flow in tissue sample 610.

Hence, system 900 and/or IR laser of one or more non-visible light sources 607, can be operated in at least two modes. In particular, the IR laser can be operated in one of a diffused mode, when optical filter 611 is filtering light to camera 609, and a speckled mode when second optical filter 911 is filtering light to camera 609. In other words, the diffuse mode can be used when operating system 900 in a manner similar to system 600.

In yet further implementations, system 900 can be used in a third mode. In particular, the IR laser can be operated in a speckled mode when second optical filter 911 is filtering light to camera 609, and the sequence of light emitted by multispectral light source 601 includes green light emitted from the green LED, and blue light emitted from the blue LED, when optical filter 611 is filtering light to camera 609, speckled laser light from the IR laser in the speckled mode, the green light and the blue light used for functional imaging of blood flow in the tissue sample. In other words in the third mode, when optical filter 611 is filtering light to camera 609, green light and blue light can be used in sequence to irradiate tissue sample 610, and then optical filters 611, 911 can be exchanged, and the IR laser can be operated in a speckled mode (though the specific sequence of colors irradiating tissue sample 610 is generally irrelevant, presuming at least one control unit 615 is synchronizing such irradiation with filter position, and image acquisition).

In yet further implementations, one or more of systems 600, 900 can be adapted to include further optical filters and further light sources. For example, in some implementations, filter wheel 912 can be adapted to include three optical filters having the following transmission characteristics:

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Filter 1: Transmits light in a visible range of about 400 nm to about 700 nm, allowing visible light reflected from tissue sample **610** to be imaged by camera **609**, and which can be used for “standard” white light surgery.

Filter 2: Transmits light in an extended range of about 400 nm to about 800 nm, allowing light from an IR laser operated in a speckled mode to be imaged by camera **609**, and which can be used for concurrent white light surgery and quantitative blood physiology measurement.

Filter 3: Transmits light in a fluorescent range of about 430 nm to about 700 nm, and from about 820 nm to about 860 nm, which blocks light from both UV and IR light sources while allowing light from the emission of PpIX & ICG from tissue sample **610** to be imaged by camera **609**.

In other words, optical filters respective to light emitted from multispectral light source **601** can be used depending on a mode of operation of the system and what wavelengths of light are being reflected and/or emitted by tissue sample **610**.

Persons skilled in the art will appreciate that there are yet more alternative implementations and modifications possible. For example, attention is next directed to FIG. **11** which depicts a system **1100** that is substantially similar to system **600**, with like elements having like numbers. However, system **1100** further comprises: a second camera **1109** arranged relative to camera **609** to acquire three-dimensional images of tissue sample **610**; hence, as depicted cameras **609**, **1109** can be angled and/or positioned to image a same region of tissue sample **610**. System **1100** further comprises a second optical filter **1111**, positioned to filter light into second camera **1109**, second optical filter **1111** configured to: transmit visible light from the LED array **605** and transmit non-visible light from one or more non-visible light sources **607** in the one or more given non-visible frequency ranges. For example, second optical filter **1111** can be configured to transmits light in a fluorescent range of about 430 nm to about 700 nm, and from about 820 nm to about 860 nm, which blocks light from both UV and IR light sources while allowing light from the emission of PpIX & ICG from tissue sample **610** to be imaged by camera **1109**; such implementations assume that the one or more non-visible light sources **607** comprises an IR laser, which can be operable in one of a diffused mode and a speckled mode, and a UV laser.

Hence, using two sets of cameras and respective optical filters, different modes of imaging tissue sample **610** can be performed simultaneously. Alternatively, camera **609** and second camera **1109** can be configured to capture images independent of one another, such that system **1100** can be operated in different modes at different times.

Persons skilled in the art will appreciate that there are yet more alternative implementations and modifications possible. For example, in some implementations, one or more of system **600**, **900**, **1100** can further comprise a thermal camera arranged to receive light from tissue sample **610** illuminated by the multispectral light source **601** in the sequence, thereby performing thermal imaging of tissue sample **610**; for example, in system **100**, camera **1109** can comprise a thermal imaging camera and optical filter **1111** can either be removed from system **1100** or adapted to transmit light in a thermal imaging range.

Furthermore, in some implementations, light sources, filters and cameras can be packaged together in an apparatus compatible for use with an access port, such as access port **12**. For example, attention is directed to FIG. **12**, which

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depicts system **600**, in which multispectral light source **601**, camera **609**, and optical filter **611** are assumed to be packaged in an apparatus **1250**, which can comprise an endoscope and the like; as depicted, apparatus **1250** has been inserted through access port **12**, depicted in cross-section.

As depicted, apparatus **1250** comprises an optional tracking device **1255** attached to a proximal end apparatus **1250**. In other words, as depicted, system **600** optionally comprises tracking device **1255** configured to be tracked by a navigation system. Tracking device **1255** is generally configured to be tracked by a navigation system external to system **600**, for example a navigation system that is part of surgical system, such as that depicted in FIGS. **1** to **4**. While not depicted apparatus **1250** can further comprise a mount configured to removably attach tracking device **1255** at a proximal end thereof (e.g. an end that is away from tissue being imaged). Tracking device **1255** is generally positioned so that a camera, and the like, of a surgical navigation system may track a position of tracking device **1255** and hence a relative position of a distal end of apparatus **1250** (e.g. an end of apparatus **1250** closest to tissue sample **610**). As depicted, tracking device **1255** comprises four reflective spheres arranged in a configuration where each sphere is located at about a corner of a square. However, other numbers of spheres and other configurations are within the scope of present implementations. In particular or more of a number, arrangement, and configuration of such spheres may be selected to provide a given tracking accuracy, including, but not limited to, a tracking accuracy that is less than about half a diameter of a sensing array surface. However, tracking device **1255** may include tracking devices other than reflective spheres. For example, in some implementations, tracking device **1255** may include a flexible sheath configured to measure tip position deflection, for example deflection of a tip of the flexible sheath. Furthermore, system **600** can be adapted to include one or more tracking devices.

Furthermore, at least one control unit **615** can comprises one or more ports configured for communicate with one or more of: surgical navigation system; external computing devices; electronic surgical devices; trackers; and infrared trackers.

Persons skilled in the art will appreciate that there are yet more alternative implementations and modifications possible. For example, at least one control unit **615** can be configured to implement various image processing algorithms including, but not limited to: amplification of the color dynamics around the edge of the tumor margin under FGS mode, image fusion between WLS and FGS modes, division of the light reflectance under blue light to that of green light for blood oxygenation and volume computations, spatial computation under speckled laser illumination for blood perfusion.

When using two cameras, which can be used for combined three-dimensional vision, as in system **1100**, image processing algorithms implemented by at least one control unit **615** can further include finding parameters to warp image from each camera onto another. In some of these implementations, at least one control unit **615** can control multispectral light source **601** to intermittently flash blue light from the blue LED into one camera and flash blue light from the blue LED into the other camera (e.g. assuming that at least one control unit **615** is synchronizing images from the cameras) to obtain a quantitative blood physiology while warping and merging images from each camera into a single image.

In yet further implementations, systems described herein can be adapted to include external sources and at least one control unit **615** can either comprise or be a component of other surgical systems and/or be in communication with a main control hub of surgical system. In such implementations, at given intervals (e.g. every second), such a main control hub cause camera acquisition of systems described herein to stop such that external source can be used to perform other imaging techniques, including, but not limited to, intraoperative Raman spectroscopy. Furthermore, when tracking devices are used with systems described herein (e.g. as depicted in FIG. **12**), and such tracking devices are tracked using light in an infrared spectrum such infrared light can introduce artefacts from pulsing infrared diodes on the acquired images unless optical filters described herein are further adapted to filter out such artefacts. For example, the sequence depicted in FIG. **8** could be modified to include an infrared tracking pulse in the 700 nm to 800 nm region between frames and/or within a frame that illuminates apparatus **1255**, which is detected by a tracking system, but images of apparatus **1255** and/or the tracking pulse, is filtered out of camera **609** using optical filter **611** (e.g. see FIG. **7**). Hence, by using system **600**, infrared tracking can be used in conjunction with FGS without introducing artefacts into images of tissue sample **610** rendered at display device **613** from camera **609**.

In yet further implementations, at least one control device **615** can be adapted to perform sub-frame synchronization, for example by controlling camera shutter speeds and/or camera “sync” pulses to stagger image acquisition on a sub-frame basis; such a feature can obviate reductions in frame rate in a global acquisition of images, for example in different spectral and/or wavelength ranges. Such a feature can also be referred to as “time multiplexing of image acquisition and illumination”, which can be used for different modalities of systems **600**, **900**, **1100** that include a plurality of cameras that can acquire images in different spectral and/or wavelength ranges. For example, systems **600**, **900**, **1100** can be used as a kind of “global image and illumination scheduler” using the mentioned sync pulses, and the like, which can ensure that the various image acquisitions in the different spectral and/or wavelength ranges (e.g. tracking, visible, non-visible, etc.) don’t interfere with each other as they all require different lighting and capture environments. For example, in a specific non-limiting example, such sub-frame synchronization could be implemented in a system comprising multiple cameras, each with a frame rate of 60 Hz; hence a frame is acquired every $\frac{1}{60}$ of a second (however, camera speeds are often faster, and such acquisitions can occur at rates on the order of every $\frac{1}{250}$ of a second to every $\frac{1}{1000}$ of a second, and faster); in such implementations, image capture times of each camera can be slightly off-set with respect to one another, and images from each camera can be acquired within the $\frac{1}{60}$ th of a second, within different spectral and/or wavelength ranges, and hence multispectral image can be acquired without reducing frame rate.

The specific embodiments described above have been shown by way of example, and it should be understood that these embodiments may be susceptible to various modifications and alternative forms. It should be further understood that the claims are not intended to be limited to the particular forms disclosed, but rather to cover all modifications, equivalents, and alternatives falling within the spirit and scope of this disclosure.

What is claimed is:

1. A multispectral synchronized imaging system, comprising:
 - a multispectral light source configured to illuminate tissue, the multispectral light source comprising:
 - a light emitting diode (LED) array configured to emit visible light including visible white light, the LED array comprising:
 - at least one blue LED configured to emit blue light,
 - at least one green LED configured to emit green light, and
 - at least one red LED configured to emit red light,
 wherein each of the at least one blue LED, the at least one green LED, the at least one red LED is individually addressable; and
 - one or more non-visible light sources configured to emit non-visible light in one or more given non-visible frequency ranges, wherein the one or more non-visible light sources:
 - are arranged side by side with the LED array,
 - are independently addressable, and
 - comprise an infrared (IR) laser, wherein the one or more given non-visible frequency ranges comprise an IR frequency range, and the non-visible light comprises IR light emitted from the IR laser,
 - a first camera arranged to capture images of the tissue by receiving light reflected from or emitted by the tissue;
 - a first optical filter and a second optical filter;
 - a filter positioning device configured to selectively position a selected one of the first optical filter and the second optical filter relative to the first camera such that the selected optical filter positioned relative to the first camera filters said light reflected from or emitted by the tissue prior to being received by the first camera, wherein, when the first optical filter, as the selected optical filter, is positioned by the filter positioning device relative to the first camera and the visible white light from the LED array illuminating the tissue reflects off the tissue, the first optical filter is configured to: transmit the reflected visible white light to the first camera;
 - wherein, when the first optical filter, as the selected optical filter, is positioned by the filter positioning device relative to the first camera and the non-visible light from the one or more non-visible light sources in the one or more given non-visible frequency ranges illuminating the tissue reflects off the tissue and excites the tissue to emit a first tissue-emitted light, the first optical filter is configured to: filter the reflected non-visible light so as to be blocked from being received by the first camera, and transmit the first tissue-emitted light to the first camera;
 - wherein, when the first optical filter, as the selected optical filter, is positioned by the filter positioning device relative to the first camera and the IR light from the IR laser illuminating the tissue reflects off the tissue and excites the tissue to emit a second tissue-emitted light, the first optical filter is configured to: filter the reflected IR light so as to be blocked from being received by the first camera, and transmit the second tissue-emitted light to the first camera; and
 - wherein, when the second optical filter, as the selected optical filter, is positioned by the filter positioning device relative to the first camera and the IR light from the IR laser illuminating the tissue reflects off

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the tissue, the second optical filter configured to:
 transmit the reflected IR light to the first camera;
 a display device;
 at least one control unit configured to:
 control the multispectral light source to emit, in a sequence, at least:
 the visible white light,
 the non-visible light, and
 simultaneously at least two or more selected from the group consisting of the blue light, the green light, and the red light,
 wherein the sequence comprises one or more user configured sequence(s);
 control the multispectral light source, the filter positioning device, and the camera in a synchronized and alternating manner to acquire first images and second images in an alternating manner wherein:
 the first images are captured by the first camera for each illumination of the tissue by multispectral light source with the blue light, the green light, the visible white light, the IR light, and the non-visible light, while the first optical filter, as the selected optical filter, is positioned by filter positioning device relative to the first camera; and
 second images are acquired for illumination of the tissue by the multispectral light source with the IR light, while the second optical filter, as the selected optical filter, is positioned by the filter positioning device relative to the first camera; and
 respectively output the first images and the second images to the display device; and
 wherein the at least one control unit is further configured to:
 enable the multispectral light source to operate in a first mode, whereby diffused IR light is emitted;
 control the filter positioning device to position the first optical filter, as the selected optical filter, relative to the first camera so as to filter the diffused IR light from the first camera while acquiring the first images, whereby the first images from the first camera comprise fluorescence imaging images;
 output the fluorescence imaging images to the display device;
 enable the multispectral light source to operate in a second mode, whereby coherent IR light is emitted;
 control the filter positioning device to position the second optical filter, as the selected optical filter, relative to the first camera so as to transmit the coherent IR light to the first camera while acquiring the second images, whereby the second images comprise functional imaging of blood flow in the tissue;
 process the first images and the second images to quantitatively measure blood flow in the tissue sample; and
 output the first images and the second images to the display device along with quantitative measurements of the blood flow.

2. The multispectral synchronized imaging system of claim 1, wherein the one or more non-visible light sources further comprises an ultraviolet (UV) light source, and wherein the first optical filter is further configured to:
 transmit light in a range of 430 nm to 700 nm, and from 820 nm to 860 nm to allow light from fluorescent emission of one or more of PpIX (Protoporphyrin IX) and ICG (Indocyanine green) administered to the tissue to be imaged by the first camera; and

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block both UV light emitted from the UV light source and reflected off the tissue and the IR light emitted from the IR laser and reflected off the tissue from entering the first camera.

3. The multispectral synchronized imaging system of claim 1, wherein the at least one control unit is further configured to:
 control the filter positioning device to position the first optical filter, as the selected optical filter, relative to the first camera so as to filter out the reflected IR light from being received by the first camera;
 control the at least one green LED and the at least one blue LED to emit, in the sequence, the green light and the blue light respectively to illuminate the tissue;
 control the first camera to acquire the first images of the tissue under illumination by the green light and the blue light; and
 process the first images to determine tissue oxygenation of the tissue sample.

4. The multispectral synchronized imaging system of claim 1, wherein the sequence comprises emitting the visible white light, and the non-visible light in an alternating manner.

5. The multispectral synchronized imaging system of claim 1, wherein the sequence further comprises emitting the visible white light, the green light, the blue light, and the non-visible light in an alternating manner.

6. The multispectral synchronized imaging system of claim 1, wherein the at least one control unit is configured to control the multispectral light source to adjust a respective relative intensity of each of the at least one blue LED, the at least one green LED, the at least one red LED to change one or more of:
 a color temperature of the visible white light; and
 a color rendering of the first images and the second images output to the display device.

7. The multispectral synchronized imaging system of claim 1, further comprising: a second camera arranged relative to the first camera to acquire three-dimensional images of the tissue,
 wherein the at least one control unit is further configured to determine parameters to warp together images captured by the first camera with images captured by the second camera.

8. The multispectral synchronized imaging system of claim 7, wherein the first camera and the second camera are configured to capture images independent of one another such that one of the first camera and the second camera captures images at times when the other of the first camera and the second camera does not capture images and vice versa.

9. The multispectral synchronized imaging system of claim 7, wherein the at least one control unit is further configured to control the first camera and the second camera such that image capture times of each of the first camera and the second camera are off-set with respect to one another such that images captured by each of the first camera and the second camera are captured within 1/60th of a second of each other.

10. The multispectral synchronized imaging system of claim 1, wherein the at least one control unit is further configured to output the first images and the second images to the display device at a rate of 12 frames per second or higher.

11. The multispectral synchronized imaging system of claim 1, wherein the first camera comprises an optical camera.

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12. The multispectral synchronized imaging system of claim 1, further comprising a thermal camera arranged to capture images by receiving the light reflected from of emitted by the tissue.

13. The multispectral synchronized imaging system of claim 12, further comprising a third optical filter disposed in relation to the thermal camera, wherein the third optical filter is configured to transmit light in a thermal imaging frequency range.

14. The multispectral synchronized imaging system of claim 1, wherein the at least one control unit comprises one or more ports, wherein the at least one control unit is configured to communicate, via the or more ports, with one or more of: external computing devices; electronic surgical devices; trackers; and infrared trackers.

15. The multispectral synchronized imaging system of claim 1, wherein the multispectral light source, the first camera, the first optical filter, the second optical filter, and the filter positioning device are packaged together for insertion through a surgical port for corridor based surgery.

16. The multispectral synchronized imaging system of claim 1, further comprising a second camera disposed and configured, in relation to the first camera, in a manner enabling one of simultaneously imaging a same region of the tissue and asynchronously imaging the same region of the tissue,

wherein the second camera is further configured to acquire three-dimensional images of the tissue, wherein the first optical filter is disposed in relation to the first camera and the second optical filter disposed in relation the second camera, and

wherein the second optical filter further configured to: transmit the visible light from the LED array reflected off the tissue; and

transmit the non-visible light from the one or more non-visible light sources in the one or more given non-visible frequency ranges reflected off the tissue,

wherein the first camera with the first optical filter and the second camera with the second optical filter respectively enable said one of simultaneously imaging the same region of the tissue sample and asynchronously imaging the same region of the tissue sample in distinct imaging modes.

17. The multispectral synchronized imaging system of claim 16, wherein the multispectral light source, the first filter, the second filter, the filter positioning device, the first camera, and the second camera are packaged together in or to form an endoscope compatible for use with an access port.

18. The multispectral synchronized imaging system of claim 17, further comprising at least one tracking device removably coupled with a proximal end of the endoscope, the at least one tracking device configured to be tracked by an external navigation system via infrared tracking, and

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wherein at least one of the first optical filter and the second optical filter is further configured to filter an artefact caused by the infrared tracking.

19. The multispectral synchronized imaging system of claim 18, wherein the at least one control unit is further configured to control illumination by the multispectral light source and capturing of images by the first camera and the second camera for sub-frame synchronization by controlling at least one of a camera shutter speed and a camera synchronization pulse to stagger image acquisition of the first camera and the second camera on a sub-frame basis, so as to effect time multiplexing of the image acquisition and the illumination.

20. The multispectral synchronized imaging system of claim 1, further comprising a second camera arranged relative to the first camera, wherein the at least one control unit is further configured to perform at least one of: communicate with at least one of:

- a surgical navigation system,
- an external computing device,
- an electronic surgical device,
- at least one tracker, and
- at least one infrared tracker;

implement at least one image processing algorithm comprising at least one of:

- an amplification algorithm for amplifying color dynamics around an edge of a tumor margin under a fluorescence guided surgery (FGS) mode,
- an image fusion algorithm for fusing imaging between a white light surgery (WLS) mode and the FGS mode,
- a division algorithm for dividing light reflectance under the blue light from light reflectance under the green light for blood oxygenation computation and volume computation,
- a spatial computation algorithm for computing speckled laser illumination for blood perfusion, and
- an algorithm for finding parameters to warp an image captured by the first camera onto an image captured by the second camera;

control the multispectral light source to intermittently flash the blue light from the blue LED and reflected by the tissue into the first camera to capture a first blue light image and flash the blue light from the blue LED and reflected by the tissue into the second camera to capture a second blue light image to obtain a quantitative blood physiology while warping and merging the first blue light image and the second blue light image into a single image; and

communicate with a main control hub of a surgical system, wherein the main control hub is configured to cause an external light source to perform intraoperative Raman spectroscopy.

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