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(54) Titre : SYSTÈME D'ADMINISTRATION DE MÉDICAMENTS POUR L'ADMINISTRATION D'AGENTS ANTIVIRAUX
(54) Title: DRUG DELIVERY SYSTEM FOR THE DELIVERY OF ANTIVIRAL AGENTS

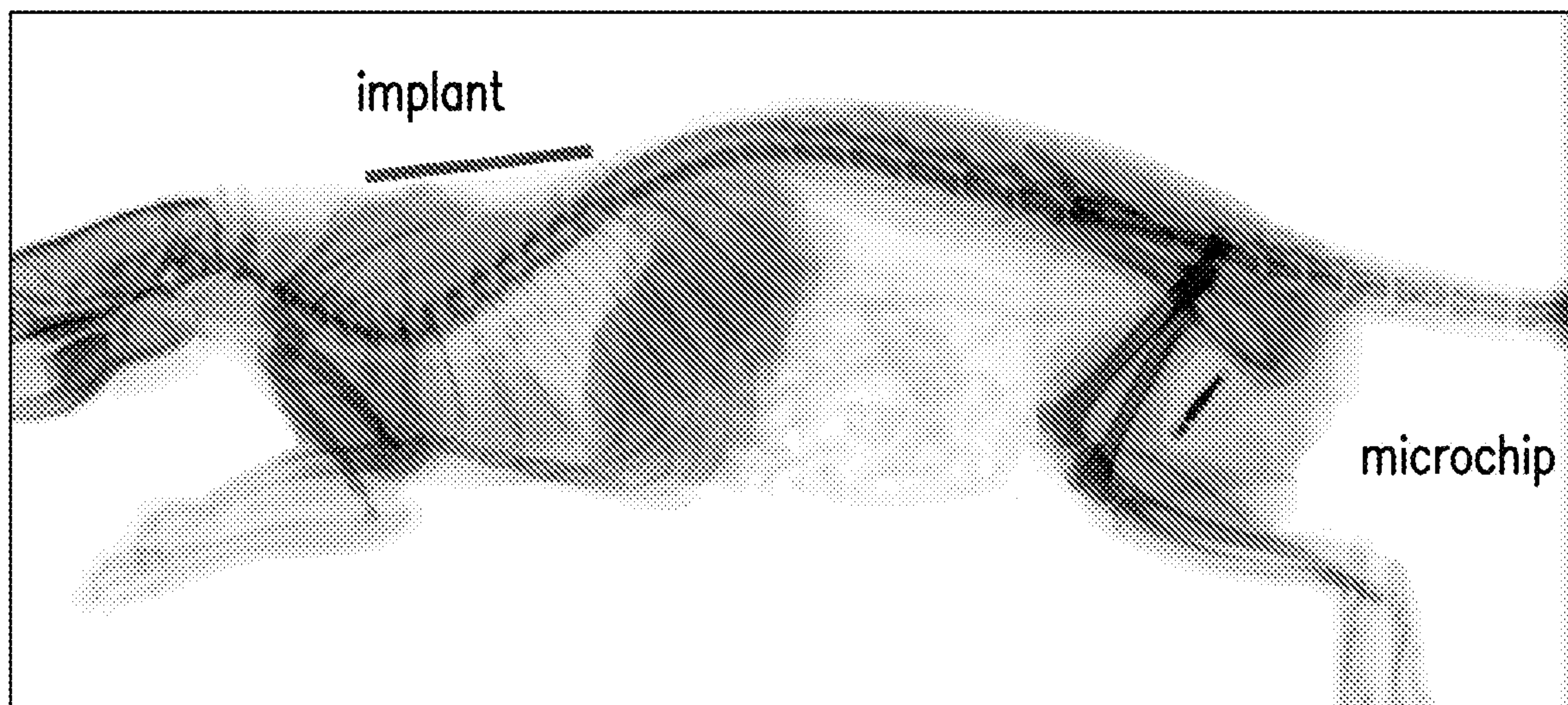


FIG. 1

(57) **Abrégé/Abstract:**

This invention relates to novel implant drug delivery systems for long-acting delivery of antiviral drugs. These compositions are useful for the treatment or prevention of human immunodeficiency virus (HIV) infection.

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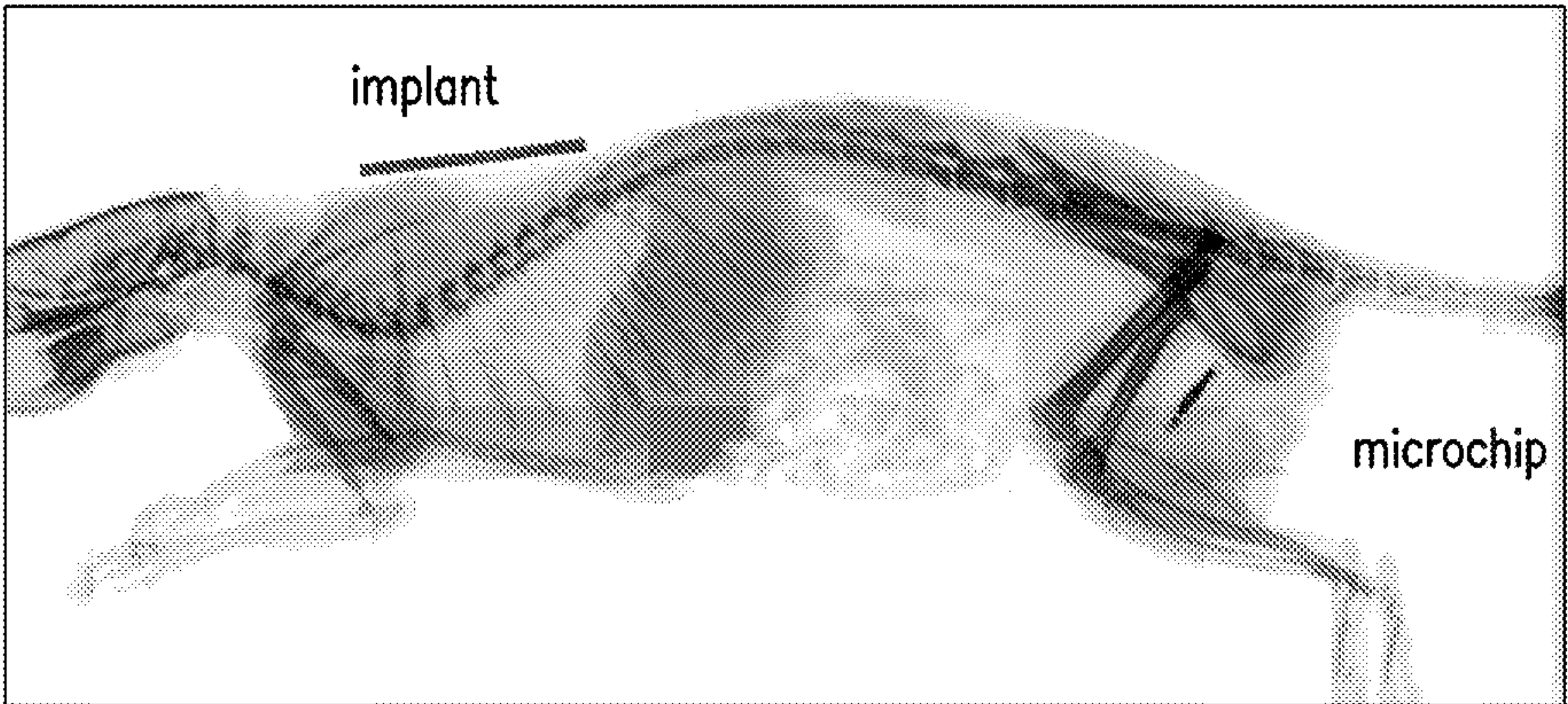


FIG. 1

(57) Abstract: This invention relates to novel implant drug delivery systems for long-acting delivery of antiviral drugs. These compositions are useful for the treatment or prevention of human immunodeficiency virus (HIV) infection.

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TITLE OF THE INVENTION

DRUG DELIVERY SYSTEM FOR THE DELIVERY OF ANTIVIRAL AGENTS

BACKGROUND OF THE INVENTION

5 The development of highly active antiretroviral therapy (HAART) in the mid 1990's transformed the clinical care of human immunodeficiency virus (HIV) type I infection. HAART regimens have proven to be highly effective treatments, significantly decreasing HIV viral load in HIV-infected patients, thereby slowing the evolution of the illness and reducing HIV-related morbidity and mortality. Yet, the treatment success of HAART is directly related to
10 adherence to the regimen by the patient. Unless appropriate levels of the antiretroviral drug combinations are maintained in the blood, viral mutations will develop, leading to therapy resistance and cross-resistances to molecules of the same therapeutic class, thus placing the long-term efficacy of treatments at risk. Various clinical studies have shown a decline in treatment effectiveness with relatively small lapses in adherence. A study by Musiime found that 81% of
15 patients with more than 95% adherence demonstrated viral suppression, while only 50% of patients who were 80–90% adherent were successful. See, Musiime, S., et al., Adherence to Highly Active Antiretroviral Treatment in HIV-Infected Rwandan Women. *PLOS one* **2011**, 6, (11), 1-6. Remarkably, only 6% of patients that were less than 70% adherent showed improvements in viral markers. Thus, low adherence is a leading cause of therapeutic failure in
20 treatment of HIV-1 infection.

Nonetheless, adherence rates to the HAART regimens continue to be far from optimal. Various characteristics of HAART make adherence particularly difficult. Therapeutic regimens are complex, requiring multiple drugs to be taken daily, often at different times of the day, and many with strict requirements on food intake. Many HAART medications also have
25 unpleasant side effects, including nausea, diarrhea, headache, and peripheral neuropathy. Social and psychological factors can also negatively impact adherence. Patients report that forgetfulness, lifestyle factors, including fear of being identified as HIV-positive, and therapy fatigue over life-long duration of treatment all contribute to adherence lapses.

New HIV treatment interventions aim to improve adherence by reducing the
30 complexity of treatments, the frequency of the dosages, and/or the side effects of the medications. Long-acting injectable (LAI) drug formulations that permit less frequent dosing, on the order of a month or longer, are an increasingly attractive option to address adherence challenges. However, the majority of approved and investigational antiretroviral agents are not

well suited for reformulation as long-acting injectable products. In large part, this is due to suboptimal physicochemical properties limiting their formulation as conventional drug suspensions, as well as insufficient antiviral potency resulting in high monthly dosing requirements. Even for cabotegravir or rilpivirine, two drugs being studied as long-acting injectable formulations, large injection volumes and multiple injections are required to achieve pharmacokinetic profiles supportive of monthly dosing. See, e.g., Spreen, W. R., et al., Long-acting injectable antiretrovirals for HIV treatment and prevention. *Current Opinion in Hiv and Aids* **2013**, 8, (6), 565-571; Rajoli, R. K. R., et al., Physiologically Based Pharmacokinetic Modelling to Inform Development of Intramuscular Long-Acting Nanoformulations for HIV. *Clinical Pharmacokinetics* **2015**, 54, (6), 639-650; Baert, L., et al., Development of a long-acting injectable formulation with nanoparticles of rilpivirine (TMC278) for HIV treatment. *European Journal of Pharmaceutics and Biopharmaceutics* **2009**, 72, (3), 502-508; Van 't Klooster, G., et al., Pharmacokinetics and Disposition of Rilpivirine (TMC278) Nanosuspension as a Long-Acting Injectable Antiretroviral Formulation. *Antimicrobial Agents and Chemotherapy* **2010**, 54, (5), 2042-2050. Thus, novel formulation approaches capable of delivering extended-duration pharmacokinetic characteristics for molecules of diverse physicochemical properties at practical injection volumes and with a limited number of injections are highly desirable.

SUMMARY OF THE INVENTION

This invention relates to novel implant drug delivery systems for long-acting delivery of antiviral drugs. These compositions are useful for the treatment or prevention of human immunodeficiency virus (HIV) infection.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1. X-ray image of a barium sulfate containing implant in a rat (image taken after a 6 month duration *in vivo*).

DETAILED DESCRIPTION OF THE INVENTION

This invention relates to novel implant drug delivery systems for long-acting delivery of antiviral drugs. The novel implant drug delivery systems comprise a polymer and an antiviral agent. These implant drug delivery systems are useful for the treatment or prevention of human immunodeficiency virus (HIV) infection. The invention further relates to methods of

treating and preventing HIV infection with the novel implant drug delivery systems described herein.

The novel implant delivery systems of the invention comprise a biocompatible nonerodible polymer to generate monolithic matrices with dispersed or dissolved drug. The chemical properties of the polymer matrices are tuned to achieve a range of drug release characteristics, offering the opportunity to extend duration of dosing. In an embodiment of the invention, the novel implant delivery systems are compatible with molecules having a broad spectrum of physicochemical properties, including those of high aqueous solubility or amorphous phases which are unsuitable to formulation as solid drug suspensions.

Specifically, this invention relates to novel implant drug delivery systems comprising a biocompatible nonerodible polymer and 4'-ethynyl-2-fluoro-2'-deoxyadenosine wherein said implant drug delivery system is implanted subdermally and 4'-ethynyl-2-fluoro-2'-deoxyadenosine is continually released *in vivo* at a rate resulting in a plasma concentration between 0.01 ng/mL and 3000.0 ng/mL. These implant delivery systems are desired and useful for prophylaxis and/or treatment of HIV infection from both compliance and convenience standpoints.

As used herein, the term "biocompatible nonerodible polymer" refers to polymeric materials that are sufficiently resistant to degradation (both chemical and physical) in the presence of biological systems. Biocompatible nonerodible polymers are sufficiently resistant to chemical and/or physical destruction by the environment of use such that the polymer remains essentially intact throughout the release period. The polymer is generally hydrophobic so that it retains its integrity for a suitable period of time when placed in an aqueous environment, such as the body of a mammal, and stable enough to be stored for an extended period before use. Nonerodible polymers remain intact *in vivo* for extended periods of time, typically months or years. Drug molecules encapsulated in the polymer are released over time via diffusion through channels and pores in a sustained manner. The release rate can be altered by modifying the percent drug loading, porosity of the polymer, structure of the implantable device, or hydrophobicity of the polymer, or by adding a coating to the exterior of the implantable device.

Accordingly, any polymer that cannot be absorbed by the body can be used to manufacture the implant drug delivery systems of the instant invention that comprise a biocompatible nonerodible polymer. Biocompatible nonerodible polymers of the instant invention include, but are not limited to, ethylene vinyl acetate copolymer (EVA),

poly(urethane), silicone, hydrogels such as crosslinked poly(vinyl alcohol) and poly(hydroxy ethylmethacrylate), acyl substituted cellulose acetates and alkyl derivatives thereof, partially and completely hydrolyzed alkylene-vinyl acetate copolymers, unplasticized polyvinyl chloride, crosslinked homo- and copolymers of polyvinyl acetate, crosslinked polyesters of acrylic acid and/or methacrylic acid, polyvinyl alkyl ethers, polyvinyl fluoride, polycarbonate, polyamide, polysulphones, styrene acrylonitrile copolymers, crosslinked poly(ethylene oxide), poly(alkylenes), poly(vinyl imidazole), poly(esters), poly(ethylene terephthalate), polyphosphazenes, and chlorosulphonated polyolefins, and combinations thereof. In a class of the invention, the biocompatible nonerodible polymer is ethylene vinyl acetate copolymer (EVA).

In a class of the invention, the biocompatible nonerodible polymer is selected from the group consisting of ethylene vinyl acetate copolymer (9% vinyl acetate), ethylene vinyl acetate copolymer (15% vinyl acetate), ethylene vinyl acetate copolymer (28% vinyl acetate), and ethylene vinyl acetate copolymer (33% vinyl acetate). In a subclass of the invention, the biocompatible nonerodible polymer is ethylene vinyl acetate copolymer (9% vinyl acetate). In a subclass of the invention, the biocompatible nonerodible polymer is ethylene vinyl acetate copolymer (15% vinyl acetate). In a class of the invention, the biocompatible nonerodible polymer is poly(urethane).

As used herein, the term “diffusional barrier” refers to a coating that is permeable to the drug and is placed over at least a portion of the device to further regulate the rate of release. For example, a coating of biocompatible nonerodible polymeric material, e.g., EVA, or a coating of a biocompatible nonerodible polymeric material with a lower drug loading than the remainder of the implant delivery system, may be used. The diffusional barrier may be formed, for example, by coextrusion with the device.

Suitable diffusional barriers of the instant invention include, but are not limited to, ethylene vinyl acetate copolymer (EVA), poly(urethane), silicone, hydrogels such as crosslinked poly(vinyl alcohol) and poly(hydroxy ethylmethacrylate), acyl substituted cellulose acetates and alkyl derivatives thereof, partially and completely hydrolyzed alkylene-vinyl acetate copolymers, unplasticized polyvinyl chloride, crosslinked homo- and copolymers of polyvinyl acetate, crosslinked polyesters of acrylic acid and/or methacrylic acid, polyvinyl alkyl ethers, polyvinyl fluoride, polycarbonate, polyamide, polysulphones, styrene acrylonitrile copolymers, crosslinked poly(ethylene oxide), poly(alkylenes), poly(vinyl imidazole), poly(esters), poly(ethylene terephthalate), polyphosphazenes, and chlorosulphonated polyolefins, and combinations thereof. In a class of the invention, the diffusional barrier is poly(urethane). In a

class of the invention, the diffusional barrier is ethylene vinyl acetate copolymer (EVA). In another class of the invention, the diffusional barrier is poly(urethane).

In an embodiment of the invention, the diffusion barrier contains an antiviral drug. In a class of the embodiment, the diffusion barrier comprises 4'-ethynyl-2-fluoro-2'-
5 deoxyadenosine.

As used herein, the term "dispersed or dissolved in the biocompatible nonerodible polymer" refers to the drug and polymer being mixed and then hot-melt extruded.

As used herein, the term "continually released" refers to the drug being released from the biocompatible nonerodible polymer at continuous rates for extended periods of time.

10 The implant drug delivery systems of the instant invention generally exhibit linear release kinetics for the drug *in vivo*, sometimes after an initial burst.

Optionally, the novel implant delivery systems of the instant invention can further comprise a radiopaque component. The radiopaque component will cause the implant to be X-ray visible. The radiopaque component can be any such element known in the art, such as
15 barium sulphate, titanium dioxide, bismuth oxide, tantalum, tungsten or platinum. In a specific embodiment, the radiopaque component is barium sulphate.

In one embodiment, the radiopaque material is about 1% to 30% by weight. In another embodiment, the radiopaque material is about 1% to 20% by weight. In another embodiment, the radiopaque material is about 4% to 25% by weight. In further embodiment, the
20 radiopaque material is about 6% to 20% by weight. In another embodiment, the radiopaque material is about 4% to 15% by weight. In another embodiment, the radiopaque material is about 8% to 15% by weight.

The radiopaque material does not affect the release of 4'-ethynyl-2-fluoro-2'-deoxyadenosine from the implant.

25 The novel implant delivery systems of the invention comprise antiviral agents. Suitable antiviral agents include anti-HIV agents. In an embodiment of the invention, the antiviral agent is administered as a monotherapy. In another embodiment of the invention, two or more antiviral agents are administered in combination.

An "anti-HIV agent" is any agent which is directly or indirectly effective in the
30 inhibition of HIV reverse transcriptase or another enzyme required for HIV replication or infection, or the prophylaxis of HIV infection, and/or the treatment, prophylaxis or delay in the onset or progression of AIDS. It is understood that an anti-HIV agent is effective in treating, preventing, or delaying the onset or progression of HIV infection or AIDS and/or diseases or

conditions arising therefrom or associated therewith. Suitable anti-viral agents for use in implant drug delivery systems described herein include, for example, those listed in Table A as follows:

Antiviral Agents for Preventing HIV infection or AIDS

Name	Type
abacavir, ABC, Ziagen®	nRTI
abacavir + lamivudine, Epzicom®	nRTI
abacavir + lamivudine + zidovudine, Trizivir®	nRTI
amprenavir, Agenerase®	PI
atazanavir, Reyataz®	PI
AZT, zidovudine, azidothymidine, Retrovir®	nRTI
Capravirine	nnRTI
darunavir, Prezista®	PI
ddC, zalcitabine, dideoxycytidine, Hivid®	nRTI
ddI, didanosine, dideoxyinosine, Videx®	nRTI
ddI (enteric coated), Videx EC®	nRTI
delavirdine, DLV, Rescriptor®	nnRTI
doravirine	nnRTI
efavirenz, EFV, Sustiva®, Stocrin®	nnRTI
efavirenz + emtricitabine + tenofovir DF, Atripla®	nnRTI + nRTI
EFdA (4'-ethynyl-2-fluoro-2'-deoxyadenosine)	nRTI
emtricitabine, FTC, Emtriva®	nRTI
emtricitabine + tenofovir DF, Truvada®	nRTI
emvirine, Coactinon®	nnRTI
enfuvirtide, Fuzeon®	FI
enteric coated didanosine, Videx EC®	nRTI
etravirine, TMC-125	nnRTI
fosamprenavir calcium, Lexiva®	PI
indinavir, Crixivan®	PI
lamivudine, 3TC, Epivir®	nRTI
lamivudine + zidovudine, Combivir®	nRTI
Lopinavir	PI
lopinavir + ritonavir, Kaletra®	PI
maraviroc, Selzentry®	EI
nelfinavir, Viracept®	PI
nevirapine, NVP, Viramune®	nnRTI
PPL-100 (also known as PL-462) (Ambrilia)	PI
raltegravir, Isentress™	InI
(S)-2-(3-chloro-4-fluorobenzyl)-8-ethyl-10-hydroxy-N,6-dimethyl-	InI
ritonavir, Norvir®	PI
saquinavir, Invirase®, Fortovase®	PI
stavudine, d4T, didehydrodeoxythymidine, Zerit®	nRTI
tenofovir DF (DF = disoproxil fumarate), TDF, Viread®	nRTI
Tenofovir, hexadecyloxypropyl (CMX-157)	nRTI

tipranavir, Aptivus®	PI
Vicriviroc	EI

EI = entry inhibitor; FI = fusion inhibitor; InI = integrase inhibitor; PI = protease inhibitor; nRTI = nucleoside reverse transcriptase inhibitor; nnRTI = non-nucleoside reverse transcriptase inhibitor.

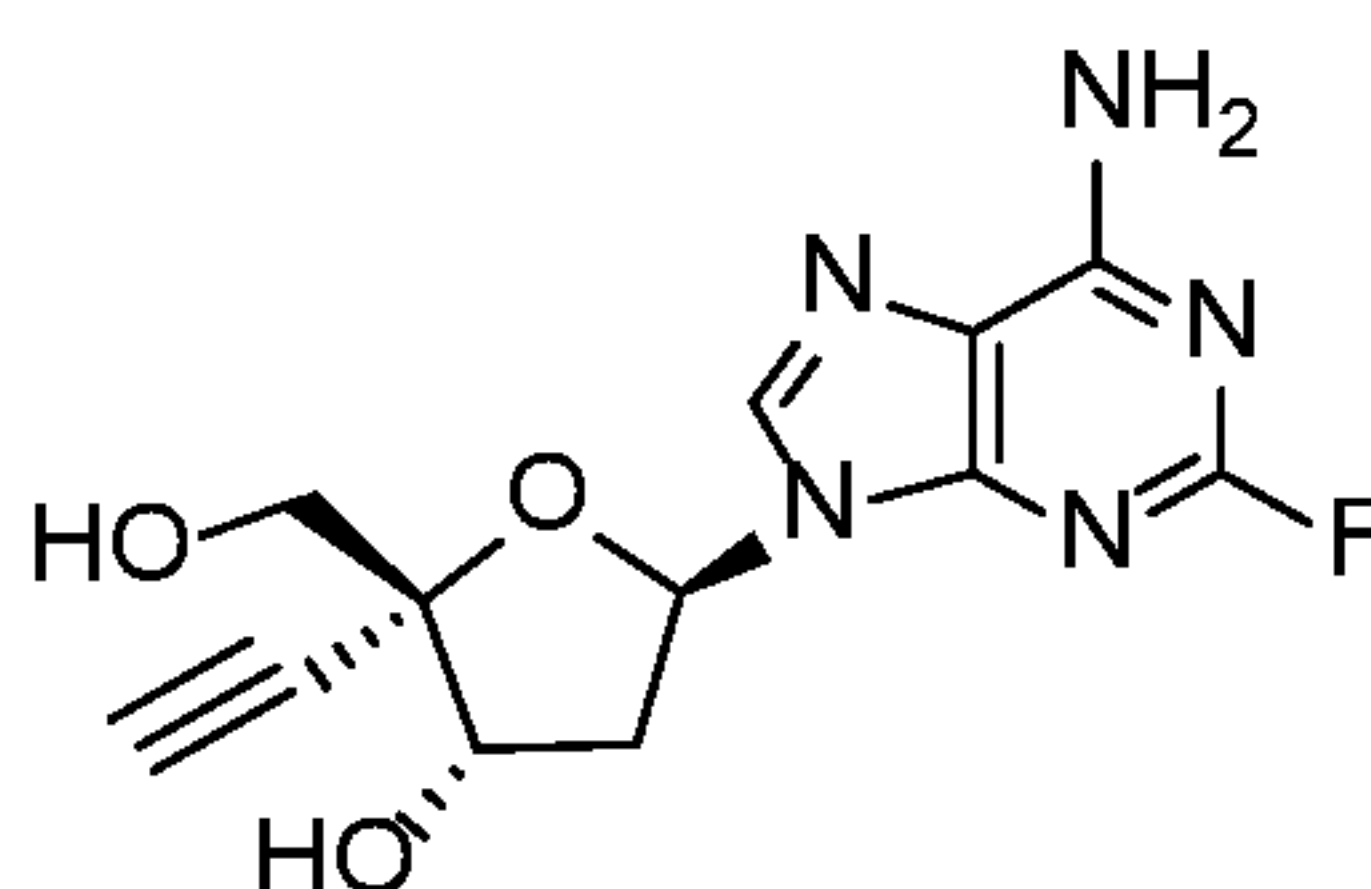
5 Some of the drugs listed in the table can be used in a salt form; e.g., abacavir sulfate, delavirdine mesylate, indinavir sulfate, atazanavir sulfate, nelfinavir mesylate, saquinavir mesylate.

10 In certain embodiments the antiviral agents in the implant drug delivery systems described herein are employed in their conventional dosage ranges and regimens as reported in the art, including, for example, the dosages described in editions of the Physicians' Desk Reference, such as the 63rd edition (2009) and earlier editions. In other embodiments, the antiviral agents in the implant drug delivery systems described herein are employed in lower than their conventional dosage ranges. In other embodiments, the antiviral agents in the implant drug delivery systems described herein are employed in higher than their conventional dosage ranges.

15 In an embodiment of the invention, the antiviral agent can be an entry inhibitor; fusion inhibitor; integrase inhibitor; protease inhibitor; nucleoside reverse transcriptase inhibitor; or non-nucleoside reverse transcriptase inhibitor. In a class of the invention, the antiviral agent is a nucleoside reverse transcriptase inhibitor.

20 In an embodiment of the invention, the antiviral agent is a nucleoside reverse transcriptase inhibitor (NRTI). In a class of the invention, the NRTI is 4'-ethynyl-2-fluoro-2'-deoxyadenosine.

4'-ethynyl-2-fluoro-2'-deoxyadenosine is also known as EFdA, and has the following chemical structure:



25 Production of and the ability of 4'-ethynyl-2-fluoro-2'-deoxyadenosine to inhibit HIV reverse transcriptase are described in PCT International Application WO2005090349, published on September 29, 2005, and US Patent Application Publication No. 2005/0215512,

published on September 29, 2005, both to Yamasa Corporation which are hereby incorporated by reference in its entirety.

In an embodiment of the implant drug delivery system described herein, the antiviral agent is present in the biocompatible nonerodible polymer at about 0.10% - 80% by weight of drug loading. In other embodiments, the antiviral agent is present in the biocompatible nonerodible polymer at about 20%-60% by weight, at about 40%-60% by weight, at about 40%-50% by weight or at about 40%-45% by weight of drug loading. In a class of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at about 0.10%-80% by weight of drug loading. In a subclass of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at about 20%-60% by weight of drug loading. In a further subclass of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at about 30%-65% by weight of drug loading. In a further subclass of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at about 40%-60% by weight of drug loading. In a further subclass of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at about 40%-50% by weight of drug loading. In a further subclass of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at about 40%-45% by weight of drug loading. In an example of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at 40% by weight of drug loading. In another example of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at 45% by weight of drug loading. In another example of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at 50% by weight of drug loading. In another example of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at 60% by weight of drug loading. In another example of the embodiment of the implant drug delivery system described herein, 4'-ethynyl-2-

fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer at 80% by weight of drug loading.

The implant drug delivery systems of the instant invention may be produced using an extrusion process, wherein ground biocompatible, nonerodible polymer is blended with the antiviral agent, melted and extruded into rod-shaped structures. Rods are cut into individual implantable devices of the desired length, packaged and sterilized prior to use. Other methods for encapsulating therapeutic compounds in implantable polymeric, nonerodible matrices are known to those of skill in the art. Such methods include solvent casting (see US Patent Nos. 4,883,666, 5,114,719 and 5,601,835). One of skill in the art would be able to readily determine an appropriate method of preparing such an implant drug delivery system, depending on the shape, size, drug loading, and release kinetics desired for a particular type of patient or clinical application.

The size and shape of the implant drug delivery systems may be modified to achieve a desired overall dosage. The implant drug delivery systems of the instant invention are often about 0.5 cm to about 10 cm in length. In an embodiment of the invention, the implant drug delivery systems are about 1.5 cm to about 5 cm in length. In a class of the embodiment, the implant drug delivery systems are about 2 cm to about 5 cm in length. In a subclass of the embodiment, the implant drug delivery systems are about 2 cm to about 4 cm in length. The implant drug delivery systems of the instant invention are often about 0.5 mm to about 7 mm in diameter. In an embodiment of the invention, the implant drug delivery systems are about 1.5 mm to about 5 mm in diameter. In a class of the embodiment, the implant drug delivery systems are about 2 mm to about 5 mm in diameter. In a subclass of the embodiment, the implant drug delivery systems are about 2 mm to about 4 mm in diameter.

The implant drug delivery systems described herein are capable of releasing 4'-ethynyl-2-fluoro-2'-deoxyadenosine over a period of 21 days, 28 days, 31 days, 4 weeks, 6 weeks, 8 weeks, 12 weeks, one month, two months, three months, four months, five months, six months, seven months, eight months, nine months, ten months, eleven months, twelve months, eighteen months, twenty-four months or thirty-six months at an average rate of between 0.02-8.0 ng per day. In an embodiment of the invention, the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is released at therapeutic concentrations for a duration from between three months and thirty-six months. In a class of the embodiment, the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is released at therapeutic concentrations for a duration from between six months and twelve months. In an embodiment of the invention, the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is released at

prophylactic concentrations for a duration from between three months and thirty-six months. In a class of the embodiment, the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is released at prophylactic concentrations for a duration from between six months and twelve months.

One or more implants can be used to achieve the desired therapeutic dose. In an embodiment of the invention, one or more implants can be used to achieve the therapeutic dose for durations of up to 1 year. In another embodiment of the invention, one or more implants can be used to achieve the therapeutic dose for durations of up to 2 years.

The implant drug delivery systems described herein are capable of releasing 4'-ethynyl-2-fluoro-2'-deoxyadenosine resulting in a plasma concentration of between 0.02-300 ng/mL per day. In an embodiment of the invention, the implant drug delivery systems described herein are capable of releasing 4'-ethynyl-2-fluoro-2'-deoxyadenosine resulting in a plasma concentration of between 0.02-30.0 ng/mL per day. In a class of the embodiment, the implant drug delivery systems described herein are capable of releasing 4'-ethynyl-2-fluoro-2'-deoxyadenosine resulting in a plasma concentration of between 0.02-15.0 ng/mL per day. In a further class of the embodiment, the implant drug delivery systems described herein are capable of releasing 4'-ethynyl-2-fluoro-2'-deoxyadenosine resulting in a plasma concentration of between 0.02-8.0 ng/mL per day. In a subclass of the embodiment, the implant drug delivery systems described herein are capable of releasing 4'-ethynyl-2-fluoro-2'-deoxyadenosine resulting in a plasma concentration of between 0.1-1.0 ng/mL per day.

The following examples are given for the purpose of illustrating the present invention and shall not be construed as being limitations on the scope of the invention.

EXAMPLE 1

PREPARATION AND IN VITRO RELEASE OF IMPLANT DRUG DELIVERY SYSTEMS

CONTAINING 30-50 WT% 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE

Implants were prepared using an extrusion process. The micronized polymer, and 4'-ethynyl-2-fluoro-2'-deoxyadenosine were blended at various ratios: 30, 35, 40, 45 and 50wt% drug in EVA. The preblend was melt extruded with a twin screw extruder at temperatures ranging from 100-140°C, screw speed at 30 rpm, and then pelletized. The pellets were then extruded with a single screw extruder with temperatures ranging from 110-140°C, and screw speed at 20-25 rpm to form a 2±0.05mm diameter filament, and then cut to a length of 40±2mm.

The *in vitro* release rate of 4'-ethynyl-2-fluoro-2'-deoxyadenosine was determined by incubating the implants segments, approximately 1 cm in length, in a glass vial

containing phosphate buffered saline (PBS) at 37°C, and 50 rpm shaking in an Innova 42 incubator. The volume of PBS was sufficient to maintain sink conditions. Sink conditions are defined as the drug concentration maintained at or below 1/3 of the maximum solubility (drug concentration $\leq$ 0.45 mg/mL in PBS at 37°C). Samples were removed (0.5 mL) at selected time points, and centrifuged at 20,800xg for 8 min. The supernatant was removed (0.4 mL), diluted 4-fold, and vortexed. Samples were assayed by HPLC (Agilent 1100 series). Analysis of a 6 μ L volume was performed at 240 nm with a Supelco Ascentis® Express C18 column (100 x 4.6 mm, 2.7 μ m). The mobile phase was 0.1% H₃PO₄ and 50:50 ACN:MeOH (83:17 v/v) at a flow rate of 1.5 mL/min (40°C).

To determine degradation of 4'-ethynyl-2-fluoro-2'-deoxyadenosine by HPLC, a 6 μ L volume was injected onto an Agilent Zorbax SB-Aq column (150 x 4.6 mm, 3.5 μ m). The mobile phase was 0.1% H₃PO₄ and 50:50 ACN:MeOH with a flow rate of 1.0 mL/min (40°C). The mobile phase gradient is shown in the table below.

Table 1. 4'-ethynyl-2-fluoro-2'-deoxyadenosine chemical stability HPLC method details

Time (min)	0.1 % H ₃ PO ₄
0.0	98
10.0	95
12.0	90
14.0	10
14.1	98
20.0	98

All samples were calibrated to 0.5 mg/mL standard solutions of 4'-ethynyl-2-fluoro-2'-deoxyadenosine in 50:50 MeOH:H₂O.

Table 2. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vitro* release from 30wt%, 35wt%, 40wt%, 45wt% and 50wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants at sink conditions; reported as a % release from total [avg = average and std dev = standard deviation]

Time (days)	30wt% EFdA + 70wt% EVA		35wt% EFdA + 65wt% EVA		40wt% EFdA + 60wt% EVA		45wt% EFdA + 55wt% EVA		50wt% EFdA + 50wt% EVA	
	avg (%)	std.dev.	avg (%)	std.dev.	avg (%)	std.dev.	avg (%)	std.dev.	avg (%)	std.dev.
0.08	0.7	0.1	1.3	0.4	1.9	0.2	2.1	0.3	2.5	0.5
0.19	0.9	0.1	1.8	0.4	2.9	0.2	3.8	0.2	4.6	0.7
0.33	1.0	0.1	2.0	0.5	3.5	0.4	4.8	0.3	5.9	0.7
0.54	1.1	0.1	2.3	0.5	4.4	0.5	6.0	0.4	7.5	1.0
1	1.3	0.2	2.7	0.6	5.6	0.8	8.0	0.6	10.5	1.3
2	1.6	0.1	3.2	0.7	7.9	1.3	12.0	0.3	16.6	2.6
3	1.7	0.2	3.5	0.7	9.2	1.5	14.5	0.5	19.8	2.8
4	1.8	0.2	3.8	0.8	10.4	1.8	17.1	0.8	23.5	3.3
8	2.2	0.3	4.7	1.1	14.4	2.5	25.1	1.4	32.3	1.8

15	2.8	0.3	6.0	1.4	20.5	3.1	35.0	2.1	44.2	2.2
23	3.4	0.4	7.2	1.7	25.3	3.8	42.8	1.8	53.5	2.2
30	3.4	0.2	7.6	2.4	28.1	5.1	46.5	1.9	57.5	1.8
37	3.6	0.4	8.4	2.2	31.4	4.4	52.3	1.8	64.6	1.7
50	4.1	0.4	9.3	2.7	35.1	4.6	59.7	1.7	72.3	0.7
59	4.6	0.5	10.2	3.1	38.8	4.8	65.3	1.9	78.4	0.3
74	5.2	0.5	11.7	3.6	44.3	5.4	73.0	2.9	85.4	0.4
84	5.3	0.5	11.8	3.7	45.4	5.0	73.6	2.2	85.9	0.1
93	5.5	0.6	12.4	4.0	47.4	5.4	76.5	2.3	88.9	0.0
102	5.7	0.6	12.8	4.1	49.9	5.6	79.2	2.8	91.2	1.7
129	5.9	0.6	13.1	4.3	51.3	5.6	78.7	2.7		
157	6.7	0.6	15.1	5.1	57.5	5.9	86.6	2.7		

Table 3. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vitro* release rates from 30wt%, 35wt%, 40wt%, 45wt% and 50wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants (normalized to a 40 mm long implant)

Sample	Release Rate at day 30 (mg/day)	Release rate at day 60 (mg/day)	Release rate at day 90 (mg/day)	Release rate at 6 months (mg/day)
30wt% EFdA + 70wt% EVA	0.03	0.02	0.02	0.01
35wt% EFdA + 65wt% EVA	0.08	0.05	0.04	0.03
40wt% EFdA + 60wt% EVA	0.30	0.21	0.17	0.12
45wt% EFdA + 55wt% EVA	0.49	0.35	0.28	0.20
50wt% EFdA + 50wt% EVA	0.67	0.48	0.39	0.27

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EXAMPLE 2

PREPARATION AND IN VITRO RELEASE OF IMPLANT DRUG DELIVERY SYSTEMS CONTAINING 50-80 WT% 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE

Implantable devices were prepared using an extrusion process. The first step involved mixing the dry, micronized powders of the active compound and the cryomilled EVA using a Turbula T2F mixer. Drug and polymer blends were prepared at 50, 60 and 80 wt % drug load. The 4'-ethynyl-2-fluoro-2'-deoxyadenosine and polymer blends were hot-melt extruded using a twin screw extruder through a 3 mm diameter die, and pulled to a diameter of approximately 1.9-2.3 mm. The screws contained predominately conveying elements with a single 90° mixing section. The 1st zone where the drug-polymer blends were introduced was water-cooled and maintained at room temperature. The temperature for zones 2-4 was 100°C .

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Extruded fibers with diameters between 1.9-2.3 mm were cut to a length of approximately 40 mm.

The *in vitro* release rate of 4'-ethynyl-2-fluoro-2'-deoxyadenosine was determined by incubating the implants segments, approximately 1 cm in length, in a glass vial containing phosphate buffered saline (PBS) at 37°C, and 50 rpm shaking in an Innova 42 incubator. The volume of PBS was sufficient to maintain sink conditions. Sink conditions are defined as the drug concentration maintained at or below 1/3 of the maximum solubility (drug concentration ≤ 0.45 mg/mL in PBS at 37°C). Samples were removed (0.5 mL) at selected time points, and centrifuged at 20,800xg for 8 min. The supernatant was removed (0.4 mL), diluted 4-fold, and vortexed. Samples were assayed by HPLC (Agilent 1100 series). Analysis of a 6 μ L volume was performed at 240 nm with a Supelco Ascentis® Express C18 column (100 x 4.6 mm, 2.7 μ m). The mobile phase was 0.1% H₃PO₄ and 50:50 ACN:MeOH (83:17 v/v) at a flow rate of 1.5 mL/min (40°C).

To determine degradation of 4'-ethynyl-2-fluoro-2'-deoxyadenosine by HPLC, a 6 μ L volume was injected onto an Agilent Zorbax SB-Aq column (150 x 4.6 mm, 3.5 μ m). The mobile phase was 0.1% H₃PO₄ and 50:50 ACN:MeOH with a flow rate of 1.0 mL/min (40°C). The mobile phase gradient is shown in table 1.

All samples were calibrated to 0.5 mg/mL standard solutions of 4'-ethynyl-2-fluoro-2'-deoxyadenosine in 50:50 MeOH:H₂O.

Table 4. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vitro* release from 50%, 60%, and 80 wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants at sink conditions; reported as a % release from total [avg = average and std dev = standard deviation]

Time (days)	50wt% EFdA + 50wt% EVA		60wt% EFdA + 40wt% EVA		80wt% EFdA + 20wt% EVA	
	avg (%)	Std. Dev.	avg (%)	Std. Dev.	avg (%)	Std. Dev.
3	10	3	18	4	38	3
7	19	2	34	4	62	3
14	27.1	0.6	49	2	93	2
21	35	1	61	3	112	1
27	37.6	0.5	65	2	106	1
35	42.6	0.4	73	2	106	1
42	45.8	0.3	79	2		
49	48.9	0.2	83	2		
63	58.9	0.3	97	2		
101	79.4	0.6				

122	83	2				
136	89.6	0.6				
149	94	1				
163	93	2				
175	97.5	0.2				

Table 5. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vitro* release rates from 50% EFdA, 60% EFdA, and 80 wt% EFdA in 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants (normalized to a 40 mm long implant) [n/d = not determined]

Sample	Release rate at day 20 (mg/day)	Release rate at day 50 (mg/day)	Release rate at day 100 (mg/day)
50wt% EFdA + 50wt% EVA	0.61	0.39	0.27
60wt% EFdA + 40wt% EVA	1.21	0.76	n/d
80wt% EFdA + 20wt% EVA	3.19	n/d	n/d

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EXAMPLE 3

PREPARATION AND IN VIVO RELEASE OF IMPLANT DRUG DELIVERY SYSTEMS CONTAINING 40, 50, 60 AND 80 WT% 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE

Implantable devices were prepared using an extrusion process. The first step involved mixing the dry, micronized powders of the active compound and the cryomilled EVA using a Turbula T2F mixer. Drug and polymer blends were prepared at 40, 50, 60 and 80 wt % drug load. The 4'-ethynyl-2-fluoro-2'-deoxyadenosine and polymer blends were hot-melt extruded using a twin screw extruder through a 3 mm diameter die, and pulled to a diameter of approximately 1.9-2.3 mm. The screws contained predominately conveying elements with a single 90° mixing section. The 1st zone where the drug-polymer blends were introduced was water-cooled and maintained at room temperature. The temperature for zones 2-4 was 100°C. Extruded fibers with diameters between 1.9-2.3 mm were cut to an appropriate length to achieve the desired amount of drug per implant for *in vivo* studies. All animal studies were conducted following protocols in accordance with the Institutional Animal Care and Use Committee (IACUC) at NIRC and Merck, which adhere to the regulations outlined in the USDA Animal Welfare Act. For each implantation, a Wistar Han rat was anesthetized using isoflurane to effect prior to subcutaneous dose administrations. Using a trocar needle, the solid formulation (~2mm in diameter and of varying lengths based on the body weight of the individual animal to achieve the dose appropriate for each group) was placed in the scapular region. Four animals (2 males

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and 2 females) were used for each formulation. Animals were monitored until recovered. At indicated time points, samples of blood were obtained from anesthetized animals (using isoflurane) and processed to plasma for determination of 4'-ethynyl-2-fluoro-2'-deoxyadenosine levels.

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Table 6. 4'-ethynyl-2-fluoro-2'-deoxyadenosine concentration in blood plasma from 40%, 50%, 60%, and 80 wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants

Time (days)	40wt% EFdA +60wt% EVA		50% EFdA +50wt% EVA		60% EFdA +40wt% EVA		80% EFdA +20wt% EVA	
	Avg. (nM)	Std. Dev. (nM)	Avg. (nM)	Std. Dev. (nM)	Avg. (nM)	Std. Dev. (nM)	Avg. (nM)	Std. Dev. (nM)
0.04	319	107	1126	356	2205	174	3722	2995
0.08	190	92	642	297	1643	350	2503	2067
0.17	105	61	317	215	1286	768	2505	2579
0.29	70	21						
1	38	16	225	115	589	81	1878	1445
2	25	11	220	37	505	68	1626	960
3	21	12	194	7	402	40	1184	424
4	17	9	179	20	379	52	1190	427
7	14	6	144	18	298	53	1162	410
10	13	5	111	19	213	27	698	202
14	9	3	91	15	197	13	428	105
17	9	2	84	10	186	13	381	93
21	5	3						
22			63	16	148	12	270	140
25			57	15	129	11	227	142
28	3	1	55	11	112	10	170	129
31	4	2	48	9	109	8	159	139
35	3	3	57	11	119	16	187	21
38			51	13	91	7	129	18
42			47	13	99	10	117	5
44	4	2						
45			45	16	85	11	66	55
51	3	2						
53			51	14	78	23		
60			36	13	64	4		
64			38	10	59	10		
65	3	1						
72	3	1						
74			37	10	55	12		
78			32	9	34	5		
79	3	1						
85			31	7	12	8		

86	3	1						
92			28	7	6	n/a		
98	3	2						
106			32	8				
113			27	7				
120			25	3				
127			25	2				
134			25	5				
141			21	5				
148			23	3				
155			19	6				
162			22	7				
169			18	4				
176			21	2				
183			18	5				
190			18	3				
197			17	3				
204			17	1				
211			15	2				
218			13	6				
225			12	8				
232			15	3				
239			13	0				
246			11	1				
253			11	0				
260			10	2				
269			8	5				

Table 7. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vivo* release rates from 40%, 50%, 60%, and 80 wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants (normalized to a 40 mm long implant)
[n/d = not determined]

Sample	Release rate at day 25 (mg/day)	Release rate at day 50 (mg/day)	Release rate at day 100 (mg/day)
40wt% EFdA + 60wt% EVA	0.014	0.012	0.009
50wt% EFdA + 50wt% EVA	0.18	0.15	0.094
60wt% EFdA + 40wt% EVA	0.39	0.25	0.036
80wt% EFdA + 20wt% EVA	0.69	n/d	n/d

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EXAMPLE 4

PREPARATION AND IN VITRO RELEASE OF IMPLANT DRUG DELIVERY SYSTEMS CONTAINING 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE WITH A RADIOPAQUE AGENT

5 Implants were prepared using an extrusion process. The micronized polymer, 4'-ethynyl-2-fluoro-2'-deoxyadenosine, and BaSO₄ were blended at various ratios: 40 and 45wt% drug in EVA, and 35 and 40wt% drug with 10wt% BaSO₄ in EVA. The preblend was melt extruded with a twin screw extruder at temperatures ranging from 100-140°C, screw speed at 30 rpm, and then pelletized. The pellets were then extruded with a single screw extruder with
10 temperatures ranging from 110-140°C, and screw speed at 20-25 rpm to form a 2±0.05mm diameter filament, and then cut to a length of 40±2mm.

 The *in vitro* release rate of 4'-ethynyl-2-fluoro-2'-deoxyadenosine was determined by incubating the implants segments, approximately 1 cm in length, in a glass vial containing phosphate buffered saline (PBS) at 37°C, and 50 rpm shaking in an Innova 42
15 incubator. The volume of PBS was sufficient to maintain sink conditions. Sink conditions are defined as the drug concentration maintained at or below 1/3 of the maximum solubility (drug concentration ≤ 0.45 mg/mL in PBS at 37°C). Samples were removed (0.5 mL) at selected time points, and centrifuged at 20,800xg for 8 min. The supernatant was removed (0.4 mL), diluted 4-
20 fold, and vortexed. Samples were assayed by HPLC (Agilent 1100 series). Analysis of a 6 µL volume was performed at 240 nm with a Supelco Ascentis® Express C18 column (100 x 4.6 mm, 2.7µm). The mobile phase was 0.1% H₃PO₄ and 50:50 ACN:MeOH (83:17 v/v) at a flow rate of 1.5 mL/min (40°C).

 To determine degradation of 4'-ethynyl-2-fluoro-2'-deoxyadenosine by HPLC, a 6 µL volume was injected onto an Agilent Zorbax SB-Aq column (150 x 4.6 mm, 3.5µm). The
25 mobile phase was 0.1% H₃PO₄ and 50:50 ACN:MeOH with a flow rate of 1.0 mL/min (40°C). The mobile phase gradient is shown in table 1.

All samples were calibrated to 0.5 mg/mL standard solutions of 4'-ethynyl-2-fluoro-2'-deoxyadenosine in 50:50 MeOH:H₂O.

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Table 8. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vitro* release from 35wt % EFdA (with 10 wt% BaSO₄), 40wt % EFdA (with and without 10wt% BaSO₄), and 45wt% EFdA in EVA implants at sink conditions

Time (days)	35wt% EFdA + 10wt% BaSO ₄ + 55wt% EVA		40wt% EFdA + 60wt% EVA		40wt% EFdA + 10wt% BaSO ₄ + 50wt% EVA		45wt% EFdA + 55wt% EVA	
	Avg (%)	std.dev.	Avg (%)	std.dev.	Avg (%)	std.dev.	Avg (%)	std.dev.
0.08	1.70	0.09	1.71	0.03	2.20	0.09	2.06	0.04
0.17	1.92	0.02	2.04	0.05	2.75	0.06	2.64	0.06
0.33	2.14	0.03	2.29	0.06	3.16	0.06	3.09	0.09
1.25	3.57	0.06	3.71	0.09	5.62	0.12	5.56	0.22
2.25	4.14	0.07	4.46	0.08	7.37	0.18	7.17	0.23
4	4.91	0.11	5.26	0.06	9.16	0.15	9.03	0.38
11	7.37	0.18	7.78	0.08	14.37	0.21	14.23	0.38
21	9.51	0.19	10.14	0.10	19.05	0.26	18.99	0.41
39	12.06	0.26	13.09	0.17	25.15	0.76	24.86	0.45
66	14.62	0.23	16.12	0.16	30.40	0.25	30.96	0.23
80	14.43	0.22	15.95	0.15	29.68	0.23	30.45	0.27
94	16.31	0.24	18.12	0.15	33.62	0.21	34.58	0.30

5 **Table 9.** 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vitro* release rates from 35wt % EFdA (with 10 wt% BaSO₄), 40wt % EFdA (with and without 10wt% BaSO₄), and 45wt% EFdA in EVA implants (normalized to a 40 mm long implant)

Sample	Release rate at day 30 (mg/day)	Release rate at day 60 (mg/day)	Release rate at day 90 (mg/day)	Release rate at 6 months (mg/day)
35wt% EFdA + 10wt% BaSO ₄ + 55wt% EVA	0.08	0.06	0.05	0.03
40wt% EFdA + 60wt% EVA	0.10	0.07	0.06	0.04
40wt% EFdA + 10wt% BaSO ₄ + 50wt% EVA	0.20	0.14	0.12	0.08
45wt% EFdA + 55wt% EVA	0.21	0.15	0.12	0.09

EXAMPLE 5

10 PREPARATION AND IN VIVO RELEASE OF IMPLANT DRUG DELIVERY SYSTEMS CONTAINING 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE WITH A RADIOPAQUE AGENT

Implants were prepared using an extrusion process. The micronized polymer, 4'-ethynyl-2-fluoro-2'-deoxyadenosine, and BaSO₄ were blended at various ratios: 40 and 45wt% drug in EVA, and 35 and 40wt% drug with 10wt% BaSO₄ in EVA. The preblend was melt

extruded with a twin screw extruder at temperatures ranging from 100-140°C, screw speed at 30 rpm, and then pelletized. The pellets were then extruded with a single screw extruder with temperatures ranging from 110-140°C, and screw speed at 20-25 rpm to form a 2±0.05mm diameter filament, and then cut to the appropriate length to achieve the desired amount of drug per implant for *in vivo* studies. All animal studies were conducted following protocols in accordance with the Institutional Animal Care and Use Committee (IACUC) at NIRC and Merck, which adhere to the regulations outlined in the USDA Animal Welfare Act. For each implantation, a Wistar Han rat was anesthetized using isoflurane to effect prior to subcutaneous dose administrations. Using a trocar needle, the solid formulation (~2mm in diameter and of varying lengths based on the body weight of the individual animal to achieve the dose appropriate for each group) was placed in the scapular region. Four animals (2 males and 2 females) were used for each formulation. Animals were monitored until recovered. At indicated time points, samples of blood were obtained from anesthetized animals (using isoflurane) and processed to plasma for determination of 4'-ethynyl-2-fluoro-2'-deoxyadenosine levels.

Figure 1 shows an x-ray image of an implant containing barium sulfate in a rat after a 6 month duration.

Table 10. 4'-ethynyl-2-fluoro-2'-deoxyadenosine concentration in blood plasma from 35wt % EFdA (with 10 wt% BaSO₄), 40wt % EFdA (with and without 10wt% BaSO₄), and 45wt% EFdA in EVA implants

Time (days)	35wt% EFdA + 10wt% BaSO ₄ + 55wt% EVA		40wt% EFdA + 60wt% EVA		40wt% EFdA + 10wt% BaSO ₄ + 50wt% EVA		45wt% EFdA + 55wt% EVA	
	avg (nM)	std.dev. (nM)	avg (nM)	std.dev. (nM)	avg (nM)	std.dev. (nM)	avg (nM)	std.dev. (nM)
0.041666667	1128	396	1418	500	2395	583	2090	303
0.083333333	592	218	715	243	1306	394	1163	228
0.166666667	228	75	271	72	505	129	502	99
1	51	14	55	12	110	13	122	22
2	32	10	36	7	71	12	95	22
9	13	3	15	4	34	5	45	4
11	10	2	15	4	32	6	43	7
16	9	2	10	2	25	5	32	4
18	9	1	9	3	23	4	31	6
23	6	2	8	3	19	4	24	4
25	6	2	7	2	18	4	22	3
30	5	2	6	1	14	3	20	3
32	5	1	6	1	14	6	18	2
37	4	1	6	1	12	3	15	4
39	5	1	5	1	12	3	15	3

44	4	1	5	1	10	3	12	2
46	4	1	5	1	10	2	13	3
51	4	1	5	2	10	3	12	2
58	3	1	4	2	9	1	11	2
65	4	2	4	0	8	2	11	2
72	3	1	4	1	9	3	11	3
79	4	2	4	1	7	2	9	3
87	4	1	3	1	7	3	10	4
93	4	2	3	1	7	2	10	4
100	3	2	3	1	6	2	9	3
107	3	1	3	1	6	1	9	2
114	4	1	3	1	6	1	9	2
121	2	1	3	1	5	2	7	2
128	2	1	2	1	4	1	7	2
135	2	1	2	1	5	2	7	2
142	2	1	2	0	5	1	8	3
149	2	1	3	1	5	1	6	2
156	2	1	2	1	4	2	6	1
163	2	1	2	1	5	2	6	1
170	2	1	3	1	4	1	7	2
177	2	1	3	1	4	1	5	1
182	2	1	2	1	3	1	6	1

Table 11. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vivo* release rates from 35wt % EFdA (with 10 wt% BaSO₄), 40wt % EFdA (with and without 10wt% BaSO₄), and 45wt% EFdA in EVA implants (normalized to a 40 mm long implant)

Sample	Release rate at day 30 (mg/day)	Release rate at day 60 (mg/day)	Release rate at day 127 (mg/day)	Release rate at 6 months (mg/day)
35wt% EFdA + 10wt% BaSO ₄ + 55wt% EVA	0.025	0.016	0.009	0.010
40wt% EFdA + 60wt% EVA	0.027	0.020	0.011	0.010
40wt% EFdA + 10wt% BaSO ₄ + 50wt% EVA	0.064	0.039	0.022	0.016
45wt% EFdA + 55wt% EVA	0.095	0.050	0.031	0.026

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EXAMPLE 6

PREPARATION AND IN VIVO STUDIES OF IMPLANT DRUG DELIVERY SYSTEMS CONTAINING 45 WT% 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE

Implants were prepared using an extrusion process. The micronized polymer, and 4'-ethynyl-2-fluoro-2'-deoxyadenosine were blended at 45wt% drug in EVA. The preblend was melt extruded with a twin screw extruder at temperatures ranging from 100-140°C, screw speed

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at 30 rpm, and then pelletized. The pellets were then extruded with a single screw extruder with temperatures ranging from 110-140°C, and screw speed at 20-25 rpm to form a 2 ± 0.05 mm diameter filament, and then cut to a length of 40 ± 2 mm.

All animal studies were conducted following protocols in accordance with the Institutional Animal Care and Use Committee (IACUC) at NIRC and Merck, which adhere to the regulations outlined in the USDA Animal Welfare Act. For each implantation, a Rhesus monkey was sedated with Ketamine HCl (100 mg/mL) prior to subcutaneous implant administrations. Using an injector device, the implant was placed subcutaneously in the interscapular region. Eight animals (4 males and 4 females) were used. Animals were monitored until recovered. At indicated time points, samples of blood were obtained and processed to plasma for determination of 4'-ethynyl-2-fluoro-2'-deoxyadenosine levels.

Table 12. 4'-ethynyl-2-fluoro-2'-deoxyadenosine concentration in blood plasma from 45wt % 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants

Time (days)	45wt% EFdA + 55wt% EVA	
	Avg (nM)	std.dev. (nM)
0.020833	237	50
0.041667	256	41
0.083333	203	25
0.166667	118	19
0.25	86	14
1	40	6
2	31	5
3	26	5
7	17	3
14	12	2
23	9	2
37	6	1
51	5	1
65	5	1
79	4	1
107	4	1
127	2.7	0.4

Table 13. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vivo* release rates from 45wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants

Sample	Release rate at day 30 (mg/day)	Release rate at day 60 (mg/day)	Release rate at day 90 (mg/day)	Release rate at 120 days (mg/day)
45wt% EFdA + 55wt% EVA	0.18	0.12	0.10	0.076

EXAMPLE 7

5 **PREPARATION AND IN VIVO STUDIES OF IMPLANT DRUG DELIVERY SYSTEMS**
CONTAINING 50WT% 4'-ETHYNYL-2-FLUORO-2'-DEOXYADENOSINE

Implants were prepared by extrusion of a 45:55 4'-ethynyl-2-fluoro-2'-deoxyadenosine:EVA at elevated temperature yielding fibers having diameters between 2.00±0.05 mm that were cut to 40±2mm for *in vivo* studies. All animal studies were conducted following protocols in accordance with the Institutional Animal Care and Use Committee (IACUC) at NIRC and Merck, which adhere to the regulations outlined in the USDA Animal Welfare Act. For each implantation, a Rhesus monkey was sedated with Ketamine HCl (100 mg/mL) prior to subcutaneous dose administrations. Using an injector device, the implant was placed subcutaneously in the interscapular region. Three animals (all males) were used.

15 Animals were monitored until recovered. At indicated time points, samples of blood were obtained and processed to plasma for determination of 4'-ethynyl-2-fluoro-2'-deoxyadenosine levels.

Table 14. 4'-ethynyl-2-fluoro-2'-deoxyadenosine concentration in blood plasma from 50wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants

Time (days)	50wt% EFdA + 50wt% EVA	
	Avg (nM)	std.dev. (nM)
0.08	117	39
0.17	86	33
0.25	74	23
1	49	3
2	33	3
9	19	4
16	13	2
30	10	2
44	8	2
58	8	1
72	8	0

86	7	1
100	6	1
114	5.2	0.8

Table 15. 4'-ethynyl-2-fluoro-2'-deoxyadenosine *in vivo* release rates from 50 wt% 4'-ethynyl-2-fluoro-2'-deoxyadenosine in EVA implants

Sample	Release rate at day 30 (mg/day)	Release rate at day 60 (mg/day)	Release rate at day 114 (mg/day)
50wt% EFdA + 50wt% EVA	0.57	0.43	0.29

WHAT IS CLAIMED IS:

1. An implant drug delivery system comprising a biocompatible nonerodible polymer and 4'-ethynyl-2-fluoro-2'-deoxyadenosine wherein said implant drug delivery system
 5 is implanted subdermally and 4'-ethynyl-2-fluoro-2'-deoxyadenosine is continually released *in vivo* at a rate resulting in a plasma concentration between 0.02 ng/mL and 300.0 ng/mL.

2. The implant drug delivery system of Claim 1 wherein the 4'-ethynyl-2-fluoro-2'-deoxyadenosine plasma concentration is between 0.02 ng/mL and 30.0 ng/mL.

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3. The implant drug delivery system of Claim 3 wherein the 4'-ethynyl-2-fluoro-2'-deoxyadenosine the plasma concentration is between 0.02 ng/mL and 8.0 ng/mL.

4. The implant drug delivery system of Claim 1 wherein the biocompatible
 15 nonerodible polymer is selected from the group consisting of ethylene vinylacetate copolymer (EVA), poly(urethane), silicone, crosslinked poly(vinyl alcohol), poly(hydroxy ethylmethacrylate), acyl substituted cellulose acetates, partially hydrolyzed alkylene-vinyl acetate copolymers, completely hydrolyzed alkylene-vinyl acetate copolymers, unplasticized polyvinyl chloride, crosslinked homopolymers of polyvinyl acetate, crosslinked copolymers of
 20 polyvinyl acetate, crosslinked polyesters of acrylic acid, crosslinked polyesters of methacrylic acid, polyvinyl alkyl ethers, polyvinyl fluoride, polycarbonate, polyamide, polysulphones, styrene acrylonitrile copolymers, crosslinked poly(ethylene oxide), poly(alkylenes), poly(vinyl imidazole), poly(esters), poly(ethylene terephthalate), polyphosphazenes, chlorosulphonated polylefins, and combinations thereof.

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5. The implant drug delivery system of Claim 4 wherein the biocompatible nonerodible polymer is ethylene vinyl acetate copolymer.

6. The implant drug delivery system of Claim 5 wherein the biocompatible
 30 nonerodible polymer is selected from the group consisting ethylene vinyl acetate copolymer (9% vinyl acetate), ethylene vinyl acetate copolymer (15% vinyl acetate), ethylene vinyl acetate copolymer (28% vinyl acetate), and ethylene vinyl acetate copolymer (33% vinyl acetate).

7. The implant drug delivery system of Claim 6 wherein the biocompatible nonerodible polymer is ethylene vinyl acetate copolymer (9% vinyl acetate).

8. The implant drug delivery system of Claim 6 wherein the biocompatible
5 nonerodible polymer is ethylene vinyl acetate copolymer (15% vinyl acetate).

9. The implant drug delivery system of Claim 4 wherein the biocompatible nonerodible polymer is poly(urethane).

10. The implant drug delivery system of Claim 1, further comprising a diffusional barrier selected from the group consisting of ethylene vinylacetate copolymer (EVA), poly(urethane), silicone, crosslinked poly(vinyl alcohol), poly(hydroxy ethylmethacrylate), acyl substituted cellulose acetates, partially hydrolyzed alkylene-vinyl acetate copolymers, completely hydrolyzed alkylene-vinyl acetate copolymers, unplasticized
15 polyvinyl chloride, crosslinked homopolymers of polyvinyl acetate, crosslinked copolymers of polyvinyl acetate, crosslinked polyesters of acrylic acid, crosslinked polyesters of methacrylic acid, polyvinyl alkyl ethers, polyvinyl fluoride, polycarbonate, polyamide, polysulphones, styrene acrylonitrile copolymers, crosslinked poly(ethylene oxide), poly(alkylenes), poly(vinyl imidazole), poly(esters), poly(ethylene terephthalate), polyphosphazenes, chlorosulphonated
20 polylefins, and combinations thereof.

11. The implant drug delivery system of Claim 10, wherein the diffusional barrier is ethylene vinyl acetate copolymer.

12. The implant drug delivery system of Claim 10, wherein the diffusional
25 barrier is poly(urethane).

13. The implant drug delivery system of Claim 1 wherein the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is dispersed or dissolved in the biocompatible nonerodible polymer.

14. The implant drug delivery system of Claim 1 wherein 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer between 0.10% to 80% by weight of drug loading.

15. The implant drug delivery system of Claim 14 wherein 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present at in the biocompatible nonerodible polymer between 30% to 65% by weight of drug loading.

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16. The implant drug delivery system of Claim 15 wherein 4'-ethynyl-2-fluoro-2'-deoxyadenosine is present in the biocompatible nonerodible polymer between 40% to 50% by weight of drug loading.

10 17. The implant drug delivery system of Claim 1 comprising between 1% and 20% by weight of a radiopaque material.

18. The implant drug delivery system of Claim 1 wherein the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is released at therapeutic concentrations for a duration from between
15 three months and thirty-six months.

19. The implant drug delivery system of Claim 1 wherein the 4'-ethynyl-2-fluoro-2'-deoxyadenosine is released at prophylactic concentrations for a duration from between three months and thirty-six months.

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20. A method of treating or preventing HIV infection with an implant drug delivery system according to Claim 1.

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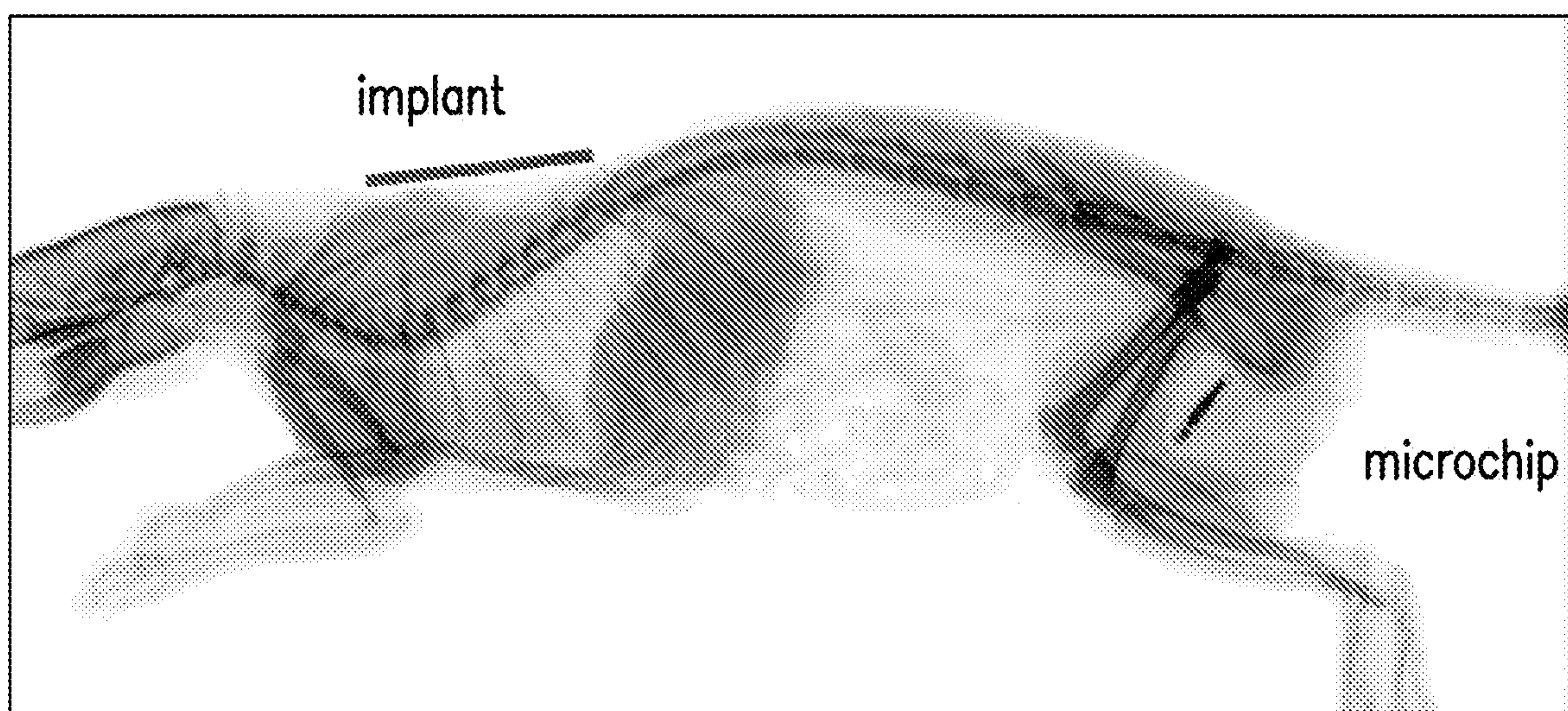


FIG. 1

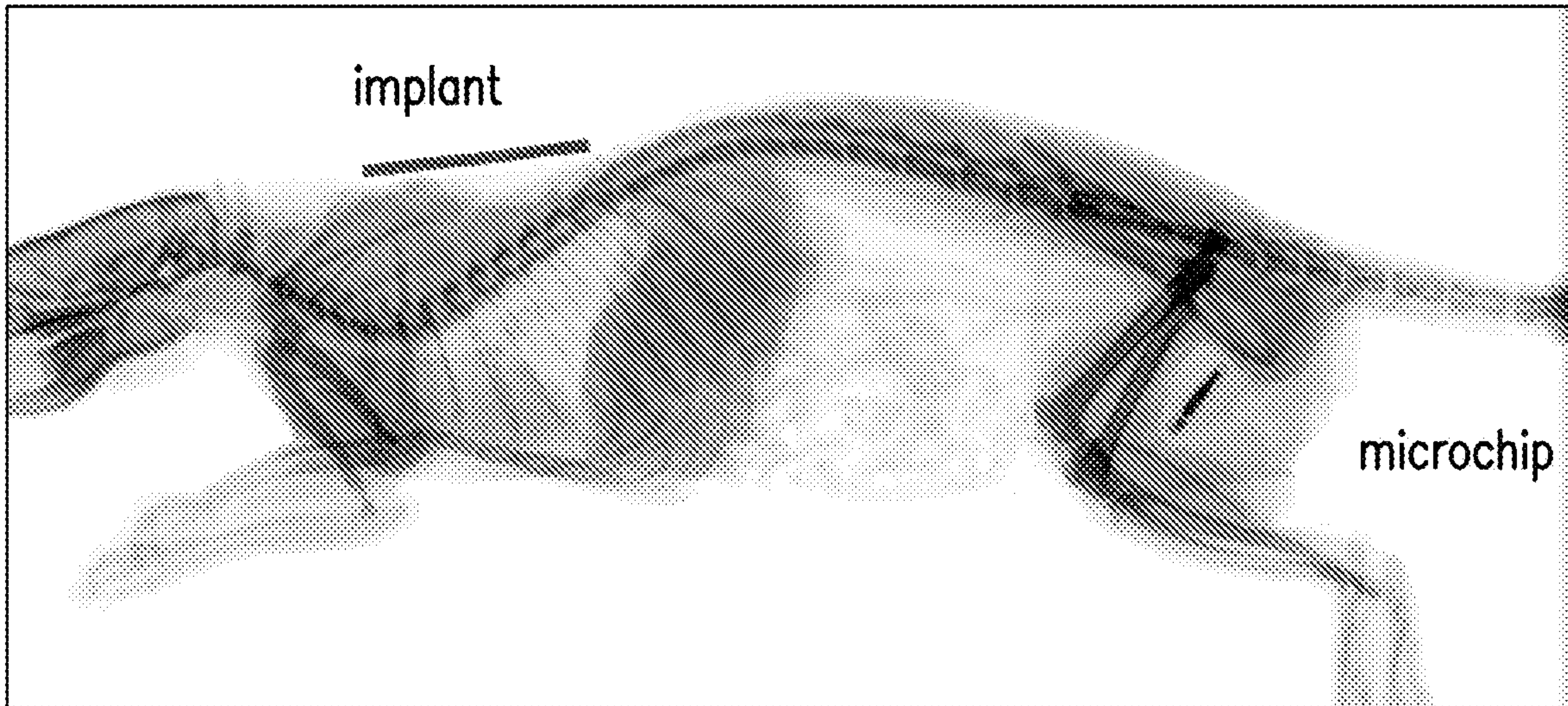


FIG. 1