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DESCRIPTION

Description

Field of the invention.

[0001] The applicant informs that the project leading to this application has received funding from the European Union's Horizon 2020 research and innovation programme under the Marie Skłodowska-Curie grant agreement No. 642458.

[0002] The searches carried out under said programme led to an invention lying in the field of the scaffolds suitable for regenerating animal tissues and of a process for producing the scaffold, the latter being in the field of the scaffolds used for repairing damaged anatomical areas in the cardio-vascular apparatus (for example the myocardium, the heart valves and blood vessels) and in the field of the so-called vascular accesses (or arteriovenous grafts), i.e. those vascular prostheses that are used to enter the blood stream via percutaneous access.

State of the art.

[0003] Scaffolds are known suitable for leading to, encouraging and supporting the regeneration of native compromised tissues. Such scaffolds are generally produced from natural materials (such as collagen, elastin, fibrin, gelatin, fibroin, chitosan, hyaluronic acid, etc.) or synthetic materials (as PCL - polycaprolactone, PGA - polyglycolic acid, PLA - polylactic acid, PTFE - polytetrafluoroethylene, PET - polyethylene terephthalate, polyurethanes, etc.) in order to confer mechanical properties adequate to those of the tissues to be replaced, on the time and in the site of implantation. With the progress in the repairing process and the consequent generation of new biological tissues, such scaffolds are usually reshaped and degraded, totally or partially, to be incorporated in or replaced by newly formed tissue.

[0004] One of the main challenges in designing a scaffold, then, is just to gather the biocompatibility properties and the mechanical properties of the material with its degradative capacities, so that the scaffold can accompany - not hinder - the repairing processes. In this context, natural materials generally appear to excel for their properties of biocompatibility, degradability and ability to reproduce the native structures, favoring the integration with host cells, while synthetic materials offer better control of mechanical properties of the scaffold, which is crucial for the application in tissues subjected to continuous mechanical stress such as those typical of the cardiovascular system. A number of attempts have been made, therefore, to combine natural materials and synthetic materials, in many forms and in different structural

organizations, in order to produce scaffolds that could afford the advantages of both classes of materials.

[0005] For example, fibroin and polyurethane scaffolds were generated, both in the form of continuous membranes and of fibrous membranes, mixing the two materials in solution or in suspension, or by the application of a fibroin coating on a polyurethane-based structure. More specifically, in the field of vascular prostheses, various technologies, such as electrospinning, dipping, gas foaming, etc., have been employed to produce hybrid tubular structures in which natural macromolecules (such as fibroin, collagen, elastin, etc.) are combined with synthetic polymers (such as polyurethanes, polyvinyl alcohol, polycaprolactone, etc.).

[0006] In the context of vascular accesses for hemodialysis, instead, grafts are commonly used to connect an arterial vessel with a venous vessel, in order to ensure the ability to perform the dialysis treatment, and they are generally composed of synthetic and non-degradable materials only, such as PTFE (polytetrafluoroethylene), polyethylene terephthalate, polyurethane. The reason for this peculiarity lies in the fact that for the arterio-venous fistulas it is critical the need to ensure sufficient mechanical properties to support the stress typical of the particular application, namely, in addition to the cyclic ones typical of the blood stream, those due to the repeated puncture by using dialysis needles.

[0007] Among the various documents in the state of the art describing scaffolds made of natural and synthetic materials, there is Patent N° CN 101214393 B that discloses a multilayer vascular prosthesis produced by electrospinning, comprising an inner layer of natural material and an outer layer made of synthetic material.

[0008] Patent N° CN 101708344 B discloses a multilayer vascular prosthesis produced by electrospinning, comprising an inner layer of natural material and an outer layer of polyurethane.

[0009] Patent N° CN 101874751 B covers a multilayer scaffold produced by "particle removal". The layers are obtained from polymeric materials (degradable and non-degradable), inorganic, biologically derived (known in the field, including fibroin among those degradable and polyurethane among those non-degradable) or mixtures thereof, and the different layers can have composition different each from the other.

[0010] Further documents found in the prior art are:

Patent application N° CN 103585674 A discloses a method for preparing a porous fibroin fiber scaffold in which a synthetic polymer material (e.g. PU) is added to the fibroin.

[0011] Document by YONGZHEN TAO ET AL: "Rheological and Mechanical Behavior of Fibroin Reinforced Waterborne Polyurethane" , POLYMERS, vol. 8, no. 3, 21 March 2016 (2016-03-21), page 94, XP55360549, DOI: 10.3390 /polym8030094 discloses the use of fibroin-reinforced polyurethane for tissue engineering.

[0012] Document by P Petrini ET AL: "Fibroin-polyurethane scaffolds for tissue engineering", Journal of Materials Science: Materials in Medicine, 1 December 2001 (2001-12-01), pages 849-853, XP55360564, Boston DOI: 10.1023/A:1012847301850 Retrieved from the Internet: URL: <https://rd.springer.com/content/pdf/10.1023/A:1012847301850.pdf> [retrieved on 2017-03-30] discloses polyurethane scaffolds having a silk-fibroin coating and their use for tissue engineering.

[0013] Patent N° CN 102499800 A discloses small-diameter vessel repairing vascular support with a PCL fibroin inner net and a middle layer sleeved with a fibroin tube.

[0014] Patent application N° CN 102817105 A discloses a method for preparing a synthetic polymer-natural polymer composite fiber with a core shell structure by coaxial electrostatic spinning. The method utilizes the synthetic polymer (e.g. polyurethane) as shell and the natural polymer (e.g. fibroin) as core.

Drawbacks in the prior art.

[0015] The greatest difficulties in the manufacture of hybrid scaffolds, composed of synthetic and natural materials, are mainly of a practical and experimental type, since often the treatments needed to process the synthetic materials (e.g. the solubilization in aggressive solvents) are detrimental for the purpose of a stable conformation of natural macromolecules, which are denatured or degraded during the process, partly losing their properties. In other cases, the treatments necessary to stabilize the natural materials (such as, in the case of fibroin, crystallization) determine in the different phases - natural and synthetic - reactions of different entities (for example, in the aforementioned case of the crystallization, volumetric shrinkage) that prevent an excellent coalescence between the materials. By the term coalescence it is intended the merging between materials (or layers of materials), due to intimate contact, binding, weaving, intersection, intermingling, or other forms of physical connection. Many attempts to cover synthetic materials with natural materials, aimed at increasing the integration of the scaffold with the host organism, then failed because of the scarce coalescence at the interface between the two materials, which determines the detachment of the coating.

[0016] Consequently, the greatest issues to be improved in the known scaffolds concern:

1. a) the integration of the scaffold with the surrounding biological tissues,
2. b) the maintenance of the intrinsic elastic properties of the synthetic polymer, that are essential for cardiovascular applications, and for applications in the field of hemodialysis vascular accesses,
3. c) the stability in combining natural and synthetic polymer, that is needed to avoid that post-processing treatments and/or operational conditions determine the delamination and/or the separation of the two materials.

[0017] As far as the above cited documents, the following deficiencies were found with respect to the above issues.

[0018] Patent application N° CN 103585674 A wouldn't solve the problem to improve the integration properties of the scaffold with the surrounding biological tissues, as the synthetic polymer would be present at the interface of the scaffold with the surrounding biological tissues, impairing the scaffold integration.

[0019] Document YONGZHEN TAO ET AL discloses a technique in which the addition of fibroin significantly affects the elastic properties of the polyurethane inducing strengthening and toughening. Moreover, the proposed solution wouldn't solve the problem to improve the integration properties of the scaffold with the surrounding biological tissues as the synthetic polymer would anyway be present at the interface of the scaffold with the surrounding biological tissues.

[0020] Document P Petrini ET AL discloses a technique in which fibroin only is present at the scaffold-tissue interface, but it fails in analyzing the effects of the fibroin coating on the mechanical properties of polyurethane foams and it surely admits that there is a mismatch of the mechanical properties of the polyurethane substrate (elastomeric) and the protein coating.

[0021] Patent N° CN 102499800 A discloses a technique which apparently succeeds in combining fibroin and PCL but no mention is made of the elastic properties of the synthetic polymer and a "suture connection" seems to be required to allow for an external tube of fibroin to improve the integration properties with the outer (not with the inner) tissues.

[0022] Patent application N° CN 102817105 A discloses a technique which indeed combines natural and synthetic material, but fails in providing the desired integration properties with the surrounding biological tissues (the synthetic material, and not the natural material is present at the interface with the surrounding tissues) and in retaining the intrinsic elastic properties of the polyurethane (no mention is made of the mechanical properties in the coaxially spun fiber).

[0023] In the specific case of hemodialysis vascular accesses, there are a number of drawbacks associated with the clinical use of prostheses made of synthetic materials:

- poor resemblance of the morphological and mechanical features of the prosthesis with those of native blood vessels;
- arising from the previous point: formation of neointimal hyperplasia at the anastomosis and subsequent stenosis or occlusion of the prosthesis and incidence of thrombotic phenomena;
- poor integration of the prosthesis with surrounding biological tissues and poor or no remodeling capacity,
- arising from the previous point: chronic inflammation in the prosthesis area.

[0024] In addition to the drawbacks recalled above, the known synthetic vascular accesses used in the hemodialysis field also suffer from:

- failure to ensure a prompt sealing of the puncture site, once the needle is removed, resulting in hemostasis delay;
- infectious phenomena.

Objects of the invention.

[0025] The invention is as defined in the appended claims. In particular, the invention refers to a method of producing a mixture of fibroin and polyurethane as defined in appended claim 1, a method for preparing a layer of fibroin and polyurethane as defined in appended claim 4 as well as the use of a combination of solvents for preparing a solution of fibroin and polyurethane as defined in appended claim 7.

[0026] The present description also refers to a scaffold made of natural and synthetic materials suitable for regenerating cardio-vascular tissues or for use as hemodialysis vascular access devoid of the prior art drawbacks and so suited to:

1. a) provide integration with the surrounding biological tissues;
2. b) retain the intrinsic elastic properties that are essential for cardiovascular applications and for applications in the field of hemodialysis vascular accesses, and
3. c) stably combine natural and synthetic materials in order to avoid that post-processing treatments and/or operational conditions cause the delamination and/or the separation of the two materials.

[0027] This object is achieved by a combination of a natural material, fibroin, with a synthetic material, a polyurethane, and conferring to the scaffold a specific multilayer structural organization.

[0028] The description further discloses how to provide scaffolds so shaped that are suitable for replacing atrioventricular or semilunar heart valves and vascular bifurcated tracts affected by pathologies.

[0029] Finally, the description discloses a process, particularly suited to industrial scale, for producing the scaffolds defined in the first object.

Background of the invention

[0030] It is started by saying that, in the following of the present description, by fibroin it is intended silk fibroin and the blood is considered to be a tissue of the animal body, and considering that "porosity" is defined as the percentage of empty space in a solid.

[0031] The first object is a hybrid scaffold produced by successively depositing, on a support of suitable shape, materials such that generate:

- peripheral layers designed to interface with the tissues in the implant site and suitable for improving the integration of the scaffold with the cells of the host organism;
- one or more intermediate layers where materials are combined to give the scaffold mechanical properties suitable to withstand the typical stresses of the implant site,

the materials being:

- fibroin for the peripheral layers,
- polyurethane combined with fibroin for each intermediate layer,

so that the scaffold comprises fibroin in the peripheral layers which confer the scaffold the property of integration with the surrounding biological tissues, and polyurethane combined with fibroin in the one or more intermediate layers that determine the stable coalescence between adjacent layers while maintaining the intrinsic elastic properties conferred to the scaffold by the polyurethane in said intermediate layers.

[0032] Indeed, applicant's direct experience confirmed that, in the absence of fibroin in the one or more intermediate layers, it is problematic to ensure coalescence between the different materials and different layers within the scaffold. In fact, as shown in the graph Fig. 5, the characteristic "Load/Extension" curve of a sample made by electrospinning a layer of fibroin, electrospinning a subsequent layer of polyurethane and then electrospinning a second layer of fibroin ("PU core" plot) showed a typical saw-toothed morphology, precisely due to delamination between layers. The applicants were able to overcome this issue, that would have impaired the integrity and the mechanical behavior of the final scaffold, only by adding fibroin to the inner layers of the scaffold (see for comparison the "SF-PU blend core" plot in the same graph, showing a neater and sharper behavior, typical of a continuum).

[0033] The structural organization, namely the shape imparted to the scaffold defined above, is of four types:

- a tubular scaffold suitable for being used as a vascular prosthesis or as a vascular access;
- a lamellar scaffold suitable for regenerating cardio-vascular tissues and in particular the myocardium;
- a shapeable scaffold of complex shape and suitable for replacing atrioventricular or semilunar heart valves or their parts, such as the annulus, valvular sinuses, flaps;

- a scaffold in the shape of bifurcated duct in one piece suitable for replacing bifurcated vascular tracts suffering conditions such as stenosis and aneurysms, for example at iliac, carotid or coronary position.

[0034] Indeed, several studies were conducted by the applicants in order to ensure the possibility to tune the mechanical properties of the scaffold to the different anatomical districts cited above. Evidences were obtained through experiments that, by varying the respective ratios of fibroin and polyurethane in the one or more intermediate layers, the scaffold elasticity can be modulated, maintaining the coalescence between the materials and the layers. As shown in the graphs depicted in Fig. 6 below, referred to electrospun meshes with intermediate layers of varied compositions (75% fibroin-25% polyurethane or 50% fibroin-50% polyurethane or 25% fibroin-75% polyurethane), increasing the polyurethane percentage allows achieving higher deformations at break, while increasing the percentage of fibroin stiffens the mesh.

[0035] The tuneability of the mechanical properties described above, besides allowing the maintenance of the intrinsic elastic properties of the polyurethane, essential for cardiovascular applications, also enables tailoring the properties of the scaffold to the specific site of implantation (e.g. cardiac valve, rather than cardiac muscle, or blood vessel), which is crucial to avoid the deleterious mismatch of elasticity between native tissues and scaffold, known to be one of the greatest causes for lack of integration of the scaffold itself.

[0036] The second object of the invention is a process in which the intermediate layer or the intermediate layers are generated from a mixture of fibroin and polyurethane (mixture prepared separately and then treated to form the scaffold).

[0037] The process used to produce the hybrid scaffold is the electrospinning that in general allows to obtain continuous filaments of nano or micrometric diameter and, in this case, allows to produce nano or micro-fibrous matrices that resemble for their effectiveness to extracellular matrix (ECM) of native tissues. With known techniques in which composite collectors are used in separate stages, the electrospinning also enables to obtain a scaffold of complex shape comprising bifurcated ducts and atrioventricular or semilunar valves.

[0038] The invented process, particularly suited to industrial scale, basically comprises:

- the electrospinning of at least a first layer of solubilized fibroin on a collector of a suitable shape for the desired scaffold;
- the subsequent deposition on the first layer of one or more intermediate layers composed of fibroin and polyurethane materials combined, by means of electrospinning a mixture of fibroin and polyurethane;
- the electrospinning of at least a last layer of solubilized fibroin, deposited on the intermediate layers or layer, said process being suitable in an industrially-sustainable context, to achieve scaffolds where fibroin and polyurethane are completely integrated, non-degraded and non-denatured.

[0039] The intermediate layers of fibroin and polyurethane are produced with the mixture of said two materials solubilized in the following conditions:

1. a) in a combination of solvents suitable for solubilizing both or each of the two materials, if necessary using additives (e.g. salts such as lithium bromide, lithium chloride, lithium iodide) to improve the solubilization of the materials;
2. b) at a concentration suitable for the porosity of the scaffold under production (lower concentration to achieve higher porosity) and for the following processing method (for example using preferably highly volatile solvents, if the mixture is then processed by electrospinning, in order to promote a better evaporation of the solvent), in a suitable weight ratio and under suitable environmental conditions (for example, by increasing the temperature above room temperature in order to promote the complete solubilization of the materials, while protecting them from denaturation and degradation);
3. c) with a sequence of operations according to the characteristics of the materials and of the solvents in use (sequence meaning the order in which the various reagents are put in contact with each other in order to avoid any precipitation of previously solubilized materials, or undesired reactions).

[0040] For example, fibroin and polyurethane in a ratio of 1:1 are solubilized in formic acid and dichloromethane in the ratio 3:2 to obtain a solution with 2% fibroin and 2% polyurethane, by solubilizing the fibroin in formic acid and the polyurethane in formic acid and dichloromethane and then combining the two solutions.

[0041] Optionally, the scaffold is subjected to known physical-chemical treatments, aimed at washing out solvent residuals and/or at inducing fibroin crystallization. The measures which may be taken are: exposure to organic solvents or to solutions of organic solvents and water or to pure water, application of mechanical stress, thermal treatments.

[0042] It should be considered that the process for the production of the scaffold was fine-tuned as a result of studies and experiments, focused on finding the best conditions to treat fibroin and polyurethane in an industrially-sustainable context, without inducing denaturation and/or degradation of the materials, and ensuring complete coalescence between them in the final scaffold.

[0043] For example, in the abovesited case of preparing a mixture of fibroin and polyurethane, several attempts were tried to avoid the use of HFP (hexafluoroisopropanol) which, despite being broadly used to simultaneously dissolve fibroin and synthetic polymers (see for example the cited documents CN 103585674 A and CN 102499800 A), is characterized by extreme volatility and high cost, thus being scarcely compatible with industrial procedures.

[0044] After several trials (e.g. with dimethylacetamide, dimethylformamide, and chloroform), it was found that a combination of solvents such as trifluoroacetic acid and dichloromethane or formic acid and dichloromethane (3:2) can solubilize both fibroin and polyurethane avoiding precipitations, denaturations and degradations, being suitable for electrospinning in an industrially-sustainable context. By using formic acid and dichloromethane (3:2), for example, evidences were found that the mixture can be processed by electrospinning to produce good-quality meshes (shown in Fig. 7) resembling native extracellular matrix, where fibroin and polyurethane are fully intermingled and completely coalescent, so as to avoid local delamination and/or detachment between the different materials.

[0045] Indeed, evidences were obtained through experiments that the invented process is also robust enough to allow for a broad variation of the fibroin/polyurethane respective ratio in the one or more intermediate layers, so as to enable the above mentioned fine tuning of the mechanical properties of the scaffold, without loss of coalescence between materials and layers. Interestingly, the changes in the respective ratios of fibroin and polyurethane in said layers did not appear to significantly affect the average stress at break of the scaffolds, confirming that the process allows for good coalescence between the two materials and integrity of the microstructure.

[0046] Such a stable coalescence between layers was found in the scaffolds also after subjecting them to crystallization treatments (e.g. in a solution of methanol and water, or in series of degrading ethanol/water solutions), assessing that the process for the production of the scaffolds allows fibroin and polyurethane to have complete coalescence, so that they in unison respond to treatments that usually determine a detachment/delamination between the two materials (due to volumetric shrinkage of fibroin and not of polyurethane upon crystallization).

[0047] Optionally, also, the inner surface of the scaffold or the entire scaffold are subjected to physical-chemical treatments, using compounds and techniques known in the field of bioengineering, in order to improve the hemocompatibility and antimicrobial properties of the scaffold itself and its permeability to blood plasma. The measures which may be taken singly or in two or more together are the following:

1. a) the inner surface of the scaffold is coated or functionalized with heparin, warfarin, statin, compounds derived from fish oil, graphite or other carbon-based compounds, anti-thrombin, argatroban, fibronectin, sulphate-based coatings, or subjected to physical processes such as gas plasma treatments and ultraviolet light, in order to improve the hemocompatibility properties.
2. b) the scaffold is completely or partly impregnated or coated with albumin or other compounds with the purpose of controlling the permeability of the blood plasma.
3. c) the scaffold is completely or partially coated or functionalized with silver, with antimicrobial peptides or antibiotic and antiviral molecules, or generated from fibroin genetically modified, in order to increase the antimicrobial properties.

Advantages of the invention.

[0048] A "constructive or process" advantage of the invention mainly resides in the fact that the industrially-sustainable treatment of the fibroin and polyurethane to produce each intermediate layer allows an excellent coalescence of the two materials within those layers themselves and with the peripheral layers that do not delaminate from each other, as in the case of the coating, nor it determines damage or denaturation of fibroin and polyurethane during processing.

[0049] In addition to this, an "operative" advantage of the invented multi-layered scaffold lies in the fact that the scaffold joins the advantages of a natural and biodegradable material (e.g. the biocompatibility, in vivo degradability, the possibility of being remodeled) with those of a synthetic and non-degradable material (e.g. the greater stability of the mechanical properties and, specifically for the polyurethane, the high elasticity). In the general case of a cardiovascular application, the polyurethane presence would improve the elasticity of the matrix, resulting in an excellent mechanical performance with respect to the typical stress in the implant site, as well as greater resistance to suture.

[0050] More specifically, in case of using the scaffold as a vascular access, the fibroin and polyurethane hybrid scaffold offers the following advantages with respect to the implants presently used in the clinics:

- thanks to the fibroin: a better reproduction of the morphological characteristics of native blood vessels, resulting in facilitating the access of the host body cells and thus in improving the integration and remodeling of the prosthesis, in a decrease of the chronic inflammation due to the implantation, in a reduction in the formation of neointimal hyperplasia at the anastomosis and, ultimately, in lower risk of stenosis and thrombosis. In this regard, it has already been shown in the scientific literature that electrospun vascular prostheses in fibroin are totally degraded and replaced by natural vascular tissue in just 7 days after implantation in an animal model (rat) [reference source Cattaneo I, Figliuzzi M, Azzollini N, V Catto, Farè S, MC Tanzi, Alessandrino A, Freddi G, Remuzzi A. In vivo regeneration of elastic lamina on fibroin biodegradable vascular scaffold. Int J Artif Organs 2013 Mar.; 36 (3): 166-74-];
- thanks to the polyurethane: a greater elasticity of the wall of the prosthesis, which allows quick sealing of the dialysis puncture site, and, consequently, a better hemostasis. In this regard, it is known that electrospun vascular prostheses in polyurethane have undoubted advantages when used as vascular access for dialysis, just for said reason,
- thanks to the fibroin: the prosthesis could enjoy moderate antimicrobial properties (this aspect being currently the object of scientific research) and thus be less susceptible to infection.

Detailed description of the invention.

[0051] The invention will now be described in detail with examples of embodiment and the help of the drawing in which:

- Figures 1- 4 are perspective/cross views.

Figure 1 shows a hybrid tubular scaffold 1 in fibroin and polyurethane suitable for being used as a vascular prosthesis or as a vascular access, of internal diameter 7 mm and length 200 mm, with the following structural organization:

- the first fibroin layer 2 has a thickness of 0.05 mm and a porosity of 60%;
- the intermediate fibroin and polyurethane layer 3 has a thickness of 0.2 mm and a porosity of 40%;
- the last fibroin layer 4 has a thickness of 0.04 mm and a porosity of 50%.

Figure 2 shows a hybrid scaffold 5 in fibroin and polyurethane in the form of a shapeable lamella, 15 mm long and 5 mm wide, suitable for regenerating vascular tissues and in particular the myocardium, with the following structural organization,

- the first fibroin layer 2a has a thickness of 0.3 mm and a porosity of 50%;
- the fibroin and polyurethane intermediate layer 3a has a thickness of 0.2 mm and a porosity of 70%;
- the last fibroin layer 4a has a thickness of 0.2 mm and a porosity of 40%.

Figure 3 shows a fibroin and polyurethane hybrid scaffolds 6 suitable for replacing an aortic valve which comprises:

- a proximal tubular part 7 suitable for connection to the ventricular myocardium, of a diameter and length congruent with those physiological in the implant anatomical site;
- an intermediate part 8 of trilobate shape resembling the natural sinuses of Valsalva in the natural valve and hosting the three valve leaflets, or valve cusps;
- a distal tubular part 9 suitable for the connection to the aorta, of diameter and length congruent with those physiological in the anatomical site of implantation,
- all three parts having in common the following structural organization:
- the first fibroin layer 2b that has a thickness of 0.05 mm and a porosity of 60%,
- the intermediate fibroin and polyurethane layer 3b which has a thickness of 0.3 mm and a porosity of 40%;
- the last fibroin layer 4b that has a thickness of 0.05 mm and a porosity of 60%.

Figure 4 shows a fibroin and polyurethane hybrid scaffolds 10 which, suitable for replacing the vascular tract called iliac bifurcation, comprises:

- a common tubular portion 11 suitable for the connection to the abdominal aorta of diameter and length congruent with those physiological of the anatomic implantation site;
- two tubular sections 12, 13 arising from the common section 11, suitable for the connection to the common iliac arteries, of diameter and length congruent with those physiological in the anatomical implantation site,
- all three parts having in common the following structural organization:
- the first fibroin layer 2c that has a thickness of 0.3 mm and a porosity of 50%,
- the intermediate fibroin and polyurethane layer 3b which has a thickness of 0.5 mm and a porosity of 40%;

- the last fibroin layer 4b that has a thickness of 0.4 mm and a porosity of 60%.

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Cited references

This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.

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Patentkrav

1. Fremgangsmåde til fremstilling af en blanding af fibroin og polyurethan, omfattende de følgende trin: solubilisere fibroin i myresyre for at opnå en første opløsning; solubilisere polyurethan til en kombination af myresyre og dichlormethan for at opnå en anden opløsning; blande den første opløsning med den anden opløsning sammen, opnå en blanding af fibroin og polyurethan opløst i en endelig opløsning af myresyre og dichlormethan, hvor nævnte endelige opløsning af myresyre og dichlormethan omfatter 3 dele af myresyre og 2 dele af dichlormethan; og

hvor nævnte fibroin solubiliseres i to dele af myresyre for at opnå nævnte første opløsning; nævnte polyurethan solubiliseres til en kombination af en del af myresyre og to dele af dichlormethan for at opnå nævnte anden opløsning; og

hvor den totale koncentration af fibroin i den endelige opløsning af myresyre og dichlormethan er i området fra 0,01 % w/v til 98,01 % w/v og den totale koncentration af polyurethan i den endelige opløsning af myresyre og dichlormethan er i området fra 0,01 % w/v til 98,01 % w/v.

2. Fremgangsmåden ifølge krav 1, hvor fibroin og polyurethan solubiliseres i den endelige opløsning af myresyre og dichlormethan i et forhold af 1:1 og en endelig opløsning opnås med 2 % w/v fibroin og 2 % w/v polyurethan.

3. Blanding af fibroin og polyurethan der kan opnås med fremgangsmåden ifølge et hvilket som helst af krav 1 til 2, hvor nævnte blanding er i form af en opløsning

4. Fremgangsmåde til fremstilling af et lag af fibroin og polyurethan, omfattende trinnene: tilvejebringe en blanding af fibroin og polyurethan i henhold til fremgangsmåden ifølge et hvilket som helst af krav 1 til 2; og elektrospinde nævnte blanding på et fibroinlag.

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5. Lag af fibroin og polyurethan, der kan opnås med fremgangsmåden ifølge krav 4.

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6. Laget ifølge krav 5, hvor sammensætningen er 75 % fibroin-25 % polyurethan eller 50 % fibroin-50 % polyurethan eller 25 % fibroin-75 % polyurethan.

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7. Anvendelse af en kombination af opløsningsmidler til fremstilling af en opløsning af fibroin og polyurethan, hvor nævnte kombination af opløsningsmidler er trifluoreddikesyre og dichlormethan eller myresyre og dichlormethan 3:2.

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8. Anvendelse ifølge krav 7, hvor kombinationen af opløsningsmidler er myresyre og dichlormethan 3:2.

DRAWINGS

Drawing

FIG. 1

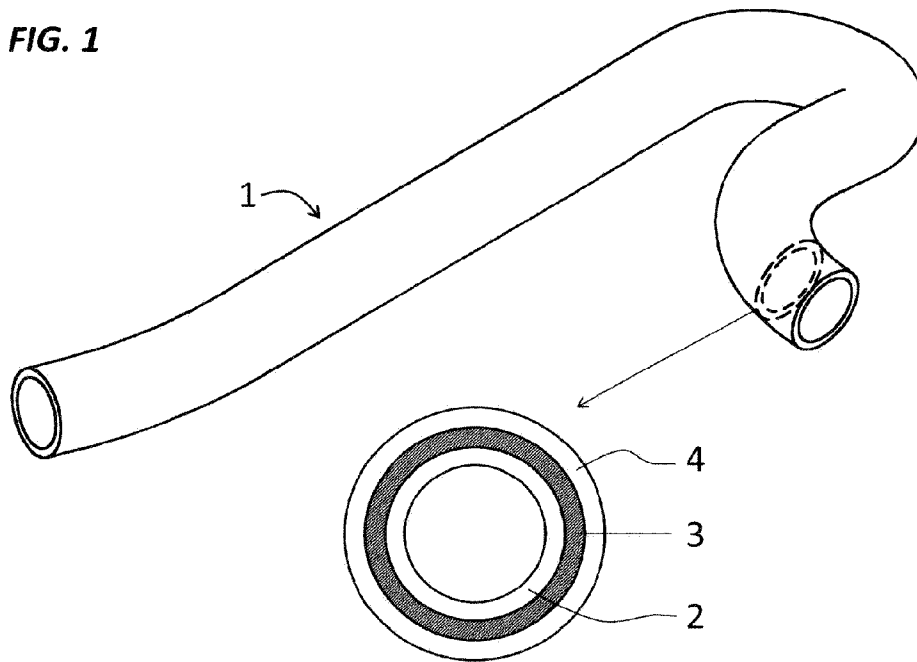


FIG. 2

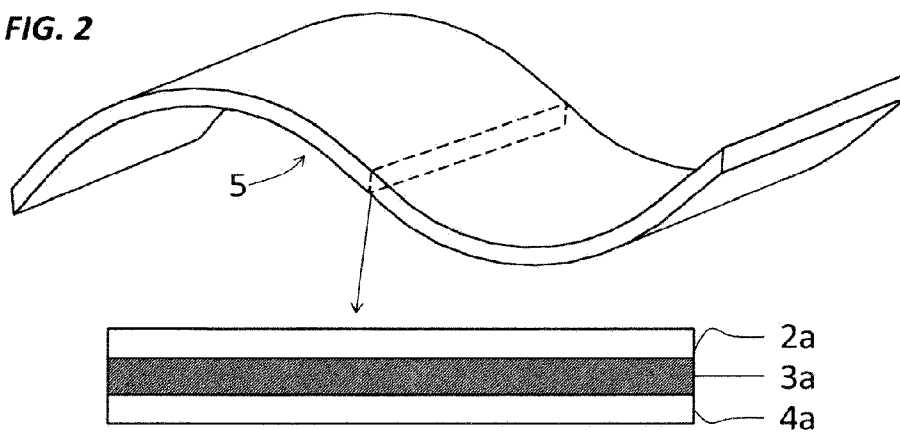


FIG. 3

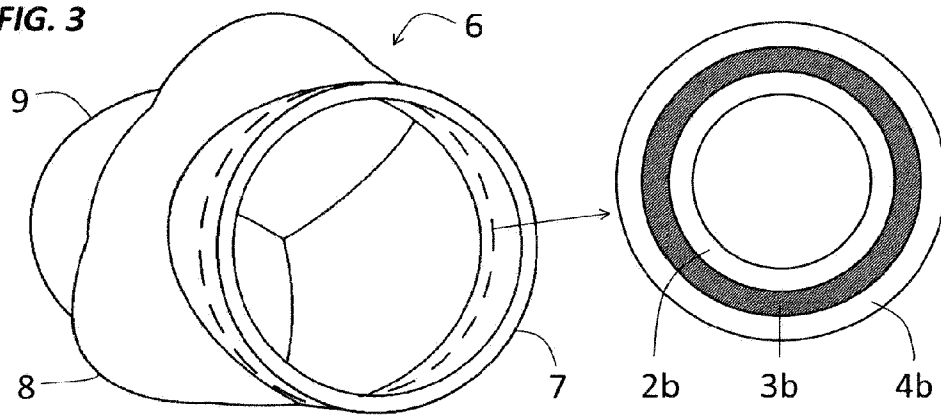
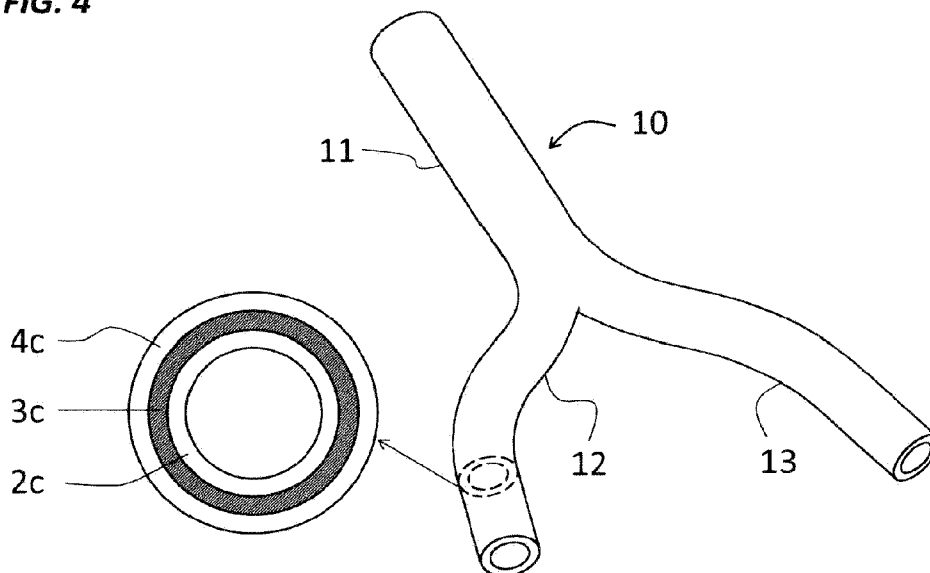
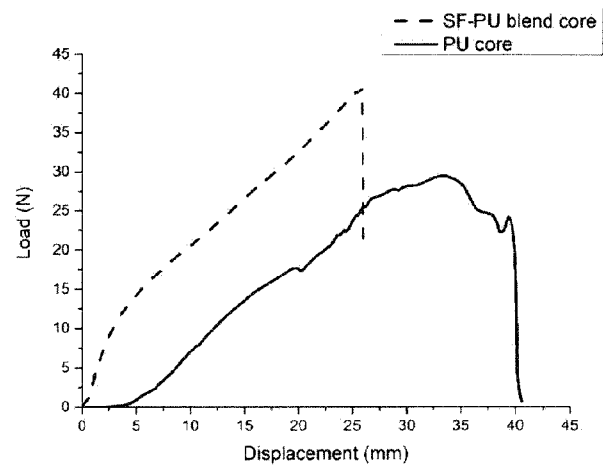
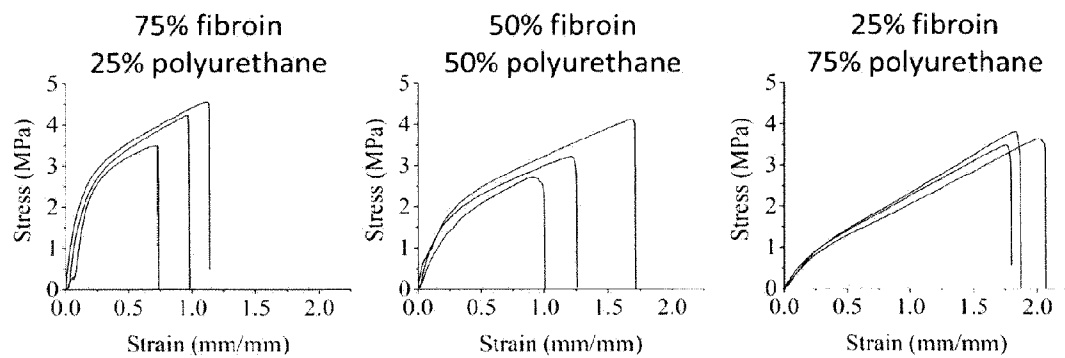


FIG. 4



**Fig. 5****Fig. 6**

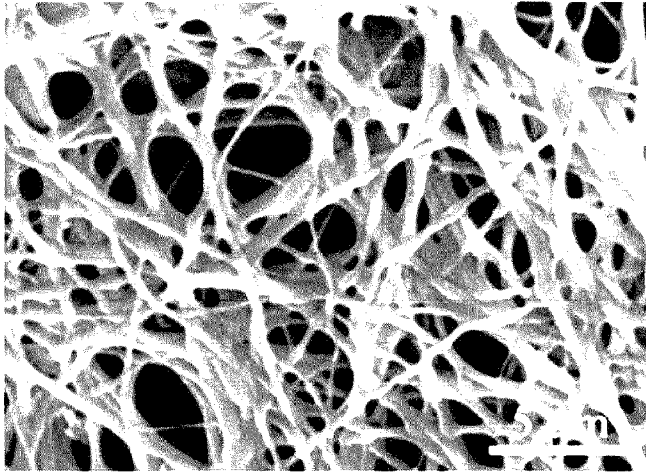


Fig. 7