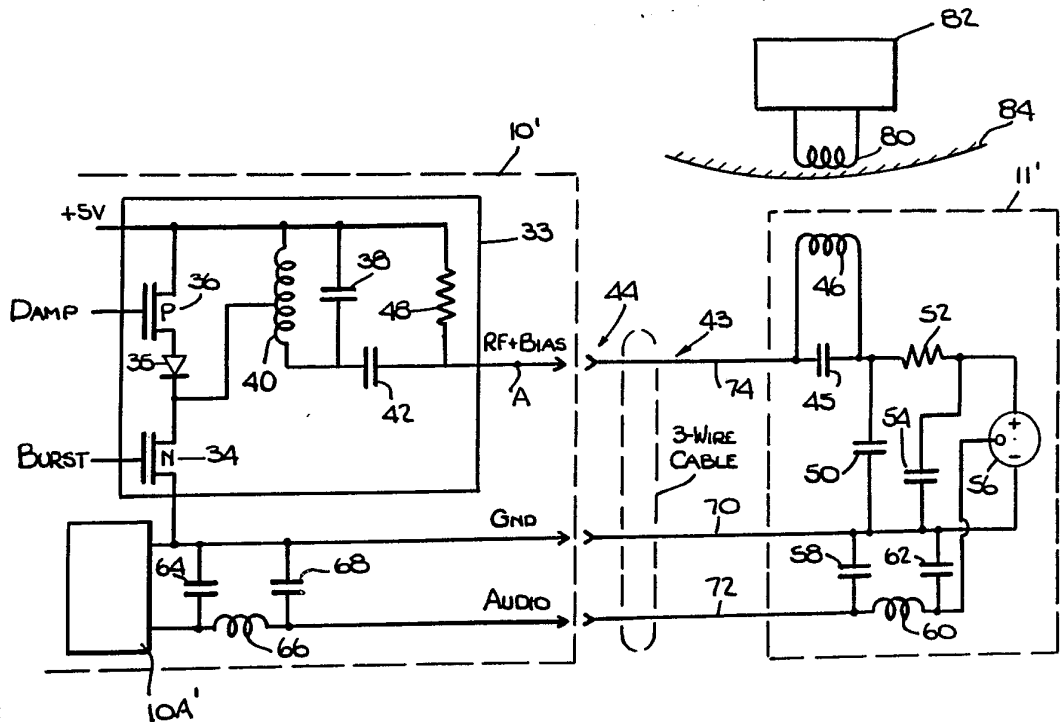




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<p>(21) International Application Number: PCT/AU90/00406 (22) International Filing Date: 7 September 1990 (07.09.90) (30) Priority data: 404,230 7 September 1989 (07.09.89) US (71) Applicant: COCHLEAR PTY. LIMITED [AU/AU]; 14 Mars Road, Lane Cove, NSW 2066 (AU). (72) Inventor: DALY, Christopher, Newton ; 95 Cheryl Crescent, Bilgola Plateau, NSW 2107 (AU). (74) Agent: MAXWELL, Peter, Francis; Peter Maxwell & Associates, Blaxland House, 5 Ross Street, North Parramatta, NSW 2151 (AU).</p>		<p>(81) Designated States: AT (European patent), BE (European patent), CH (European patent), DE (European patent)*, DK (European patent), ES (European patent), FR (European patent), GB (European patent), IT (European patent), JP, LU (European patent), NL (European patent), SE (European patent). Published <i>With international search report.</i></p>

(54) Title: THREE WIRE SYSTEM FOR COCHLEAR IMPLANT PROCESSOR



(57) Abstract

A transmission system wherein a transmitter includes a first tuned circuit (38, 40) and a transmitter coil (46) is part of a second tuned circuit (45, 46). A coupling means (42) couples energy between the first tuned circuit (38, 40) and the second tuned circuit (45, 46). A three wire unshielded cable (43) carries both radio frequency and audio frequency signals. Filter means (64, 66, 68) are provided for filtering the audio frequency signal so that it is free of interference from the radio frequency signal, which may include audio components due to its generally pulsed nature. The circuit may be adjusted for relatively constant coupling to a receiving coil (80) as separation between the transmitter coil (46) and the receiving coil changes (80).

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1 THREE WIRE SYSTEM FOR COCHLEAR IMPLANT PROCESSOR

2

3 TECHNICAL FIELD

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5 This invention relates to the field of signal
6 transmission for cochlear implant systems. More particu-
7 larly it relates to a system for transmitting both audio and
8 radio frequency energy in a multiconductor cable.

8

9 BACKGROUND OF THE INVENTION

10 The speech processor for the cochlear implant is a
11 body worn device which receives audio signals from an ear
12 level microphone and transmits an encoded RF signal to the
13 implanted device via a coil located over the implant site.
14 Thus, there is a requirement to transfer a low level audio
15 signal (typically 1 millivolt RMS) from the microphone to
16 the speech processor and a high level signal (approximately
17 10 volts RMS) back to the coil. This represents an ampli-
18 tude difference of 80 dB.

19 The high level signal is generally a modulated RF
20 carrier which typically includes frequency components in the
21 audio frequency range. The low level signal is an audio
22 signal with a bandwidth of interest of 100 Hz to 10 KHz.
23 The high level RF signal, if burst width modulated, has
24 significant frequency components within the audio spectrum.
25 It is therefore necessary to take special precautions to
26 minimize crosstalk between the two signals. In the past
27 this has been achieved by the use of a custom made multicore
28 screened cable, which provided independently shielded
29 conductors for the microphone connections and lower
30 capacitance conductors for the transmitter coil connections.
31 While this achieves the necessary isolation between the two
32 signals, it requires a special cable which is heavier than
33 ideal and very expensive to manufacture and to terminate to
34 connectors.

35

36 Body worn hearing aids have made use of a light
weight three wire twisted cable which is both readily avail-

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1 able and inexpensive. Several manufacturers provide
2 standard length cables terminated with standardized three
3 pin IEC plugs. These cables are relatively low in capaci-
4 tance, but are not screened. However, because of the above-
5 mentioned crosstalk difficulties, the audio and RF circuits
6 used in prior art cochlear implant systems cannot utilize
7 only three unshielded conductors.

8 FIG. 1, illustrates a prior art five wire system
9 for connection of a processor 10 having an audio signal
10 processing circuit 10A to a headset 11. An RF transmitter
11 12, within processor 10, operates in class-E mode, i.e. the
12 driver transistor 13, which is connected in series with a
13 diode 14 and a damping transistor 16, conducts for approxi-
14 mately fifty percent of the total cycle and switches when
15 the voltage across it is close to zero. A transmitter coil
16 18 and a capacitor 20 form a tuned circuit, which is con-
17 nected to transmitter 12 by conductors 22A and 22B of five
18 wire cable 23.

19 A microphone 22 is connected to audio signal pro-
20 cessing circuit 10A of processor 10 via an independently
21 shielded three wire portion 28 of cable 23. Cable 23
22 includes a power conductor 29A and audio conductor 29B,
23 shielded by a braid 29C connected to a ground conductor 29D.
24 A D.C. bias supply is filtered by a resistor 30 and a capa-
25 citor 31 to minimize noise of power supply origin. A five
26 wire connector 32, which is generally fairly expensive, is
27 used to connect cable 23 to processor 10.

28 The waveforms associated with the circuit of FIG.
29 1 are illustrated in FIGS. 2A to 2D. The BURST waveform of
30 FIG. 2A is applied to the gate of transistor 13. The NDAMP
31 waveform of FIG. 2B (the logical opposite of a damp wave-
32 form) is applied to the gate of transistor 16.

33 As illustrated in FIG. 2C, during the cycle, cur-
34 rent in coil 18 changes approximately linearly from a peak
35 negative value to a peak positive value. During the half
36 cycle in which transistor 13 is turned off, current cycles

- 3 -

1 sinusoidally from a peak positive value back to a peak nega-
2 tive value. As illustrated in FIG. 2D, the voltage waveform
3 across the wires 22A and 22B and coil 18 is asymmetrical,
4 swinging from -5 volts to +25 volts around the +5 volt
5 supply, during the on and off times, respectively, of driver
6 transistor 13. This extreme asymmetry in coil drive wave-
7 form results in significant low frequency components which
8 are readily coupled into the audio signal processing circuit
9 10A.

10 The mutual coupling between transmitter coil 18
11 and a receiver coil (not shown in FIG. 1) increases as the
12 distance between them decreases. The load across trans-
13 mitter coil 18 increases accordingly, and this results in
14 increased power to the transmitter. Ideally, the power
15 consumption should decrease as the coupling increases.

16 As illustrated in FIG. 3, the five wire system of
17 FIG. 1, which uses the transmitter coil as the inductor in
18 the class-E stage, exhibits characteristics opposite the
19 ideal, whereby closer coupling reflects a lower impedance
20 across the coil. This results in more energy being taken
21 from the tuned circuit and consequently the transmitter
22 draws more power.

23 Another disadvantage of the five wire system
24 illustrated in FIG. 1 is that it is necessary to have a +/-5
25 volt power supply. Such a dual voltage power supply adds
26 considerable cost to the system.

27 Prior attempts to achieve better efficiency have
28 used stagger tuning of the transmitter and a receiver using
29 a fixed transmitter frequency, or a self oscillating trans-
30 mitter circuit which detunes as coupling coefficient in-
31 creases. This latter approach is not usable with a fixed
32 frequency transmitter which is preferred for the encoded
33 pulsatile stimulation strategy.

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1 SUMMARY OF THE INVENTION

2 It is an object of this invention to use a three
3 wire twisted cable, of the type used with hearing aids, to
4 transfer both low level audio signals and high level modu-
5 lated RF signals with minimum crosstalk.

6 It is another object of this invention to improve
7 the efficiency of energy transfer from the external trans-
8 mitter system to an implanted receiver stimulator.

9 It is still another object of this invention to
10 achieve operation of the transmitter circuit from a single
11 voltage supply.

12 In accordance with the invention, a transmission
13 system for transmitting audio and radio frequency energy
14 comprises a three-wire unshielded cable; a radio frequency
15 source connected to a first wire and second wire of the
16 three wire cable; an audio frequency source connected to the
17 second wire and a third wire of the three wire cable; and
18 radio frequency filter means for filtering audio from the
19 audio source to reduce interference from the radio frequency
20 source. The filter means is disposed at at least one end of
21 the cable, and is preferably a pi network at each end.
22 Radio frequency energy from the radio frequency source is at
23 a voltage level several orders of magnitude higher than the
24 voltage from the audio frequency source. The radio fre-
25 quency source is preferably a pulsed and damped transmitter.
26 The transmitter preferably includes a class-E amplifier to
27 enhance efficiency.

28 In accordance with the invention, the transmission
29 system finds application in a cochlear implant speech pro-
30 cessor wherein the audio source is a microphone for re-
31 ceiving ambient audio. The microphone and a transmitter
32 coil associated with the transmitter are located proximate
33 to one another. The three wire unshielded cable has a first
34 end and a second end. A radio frequency transmitter circuit
35 is connected to a first wire and a second wire of the three
36 wire cable at a first end thereof. A radio frequency

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1 transmitter coil is coupled to the first wire and the second
2 wire of the three wire cable at the second end thereof. The
3 audio frequency source, which is a microphone, is coupled to
4 the second and third wires of the three wire cable at the
5 second end thereof. An audio frequency processing means for
6 processing audio from the audio frequency source is coupled
7 to the second wire and the third wire of the cable at the
8 first end thereof. A filter means for filtering the audio
9 frequency energy from the microphone so that it is essen-
10 tially free of radio frequency energy from the radio fre-
11 quency transmitter circuit is provided.

12 The invention also contemplates a radio frequency
13 transmission system having a transmitter with a first tuned
14 circuit, a transmitter coil which is part of a second tuned
15 circuit, and coupling means for coupling radio frequency
16 energy from the first tuned circuit to the second tuned
17 circuit. The coupling means may include a capacitor. The
18 first tuned circuit includes a coil which may have a tap.
19 The radio frequency driver, which includes at least one
20 active device, connects to the coil at its end or at a tap,
21 depending on the power level required and the supply
22 voltage. One side of a capacitor coupling means is
23 connected to one side of the coil and the other side is
24 connected to the second tuned circuit.

25 In a radio frequency transmission system having a
26 transmitter with a first resonant circuit, a transmitter
27 coil which is part of a second resonant circuit separate and
28 apart from the first resonant circuit and coupling means for
29 coupling energy between the first resonant circuit and the
30 second resonant circuit, the invention also contemplates a
31 method for adjusting the power transferred to a receiving
32 coil. The method comprises the steps of placing the trans-
33 mitter coil at a minimum separation from the receiving coil;
34 adjusting for resonance in the first resonant circuit so
35 that the transmitter draws minimum power; separating the
36 transmitter coil and the receiving coil to a maximum separa-

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1 tion; and adjusting the coupling means to couple sufficient
2 energy for reliable transmission to occur at the maximum
3 separation. This procedure may be used iteratively to
4 achieve optimum performance.

5 Preferably, the step of adjusting for resonance in
6 the first resonant circuit is accomplished by adjusting a
7 value of a capacitor. The coupling means is also a capa-
8 citor and the step of adjusting the coupling means comprises
9 changing a value of that capacitor. The step of separating
10 the transmitter coil and the receiver coil to a maximum
11 separation comprises separation to a maximum distance or to
12 a maximum misalignment.

13 The receiver coil is associated with a cochlear
14 implant while the transmitter coil is associated with a
15 cochlear speech processor. In the step of placing the
16 receiver coil, the minimum distance is defined by placing
17 the transmitter coil coaxially over the receiver coil.

18

19 BRIEF DESCRIPTION OF THE DRAWINGS

20 Further objects, features and advantages of the
21 invention will become apparent upon consideration of the
22 following detailed description in conjunction with the draw-
23 ings in which:

24 FIG. 1 is a schematic diagram of a prior art five
25 wire transmission system;

26 FIGS. 2A to 2D are timing diagrams of waveforms
27 associated with the circuit of FIG. 1;

28 FIG. 3 is a graph of the coupling performance of a
29 prior art five wire transmission system;

30 FIG. 4 is a schematic diagram of a three wire
31 transmission system in accordance with the invention; and

32 FIG. 5 is a graph of the coupling performance of a
33 system in accordance with the invention as illustrated in
34 FIG. 4.

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1 DESCRIPTION OF THE PREFERRED EMBODIMENT

2 Referring to FIG. 4, a transmission system in
3 accordance with the invention includes a speech processor
4 10' and a headset 11'. Speech processor 10' includes a
5 transmitter circuit 33 and an audio signal processing cir-
6 cuit 10A'. Transmitter circuit 33 includes a driver
7 transistor 34, a diode 35, and a damping transistor 36.
8 Transistor 34 is an N-channel enhancement mode MOSFET with
9 an on-resistance preferably less than five ohms for effi-
10 cient operation of the transmitter. Transistor 36 is a P-
11 channel enhancement mode MOSFET with an on-resistance of
12 less than ten ohms. Both transistors have threshold
13 voltages of less than 2.5 volts and can be driven directly
14 from typical output drives of CMOS integrated circuits.
15 They should have a voltage rating of at least 60 volts.
16 Typical industry parts for transistors 34 and 36 are VN0610L
17 and VP0610L, respectively.

18 Transmitter circuit 33 is of class-E design and
19 operates with its own tuned circuit including a capacitor 38
20 and an inductor 40, the output of which is capacitively
21 coupled by capacitor 42 to a three wire cable 43 (by a three
22 pin electrical connector 44) and a tuned transmitter circuit
23 including capacitor 45 and coil 46. Capacitor 45 must have
24 a high quality dielectric, such as that of an NPO type capa-
25 citor. The tuned circuits are close to resonance at the
26 transmission frequency, which in the preferred embodiment is
27 at 2.5 MHz.

28 The voltage and current waveforms at drive tran-
29 sistor 34 are of the same form as those for the previously
30 described five wire system illustrated in FIGS. 2A to 2D.
31 Tuned inductor 40 is tapped to provide the necessary voltage
32 gain and impedance transformation to drive transmitter coil
33 46. This is not an intrinsic feature of the design, but is
34 necessary in order to achieve adequate power output to a
35 prior existing transmitter coil, when operating from a
36 single +5 volt supply, instead of the prior +/-5 volt supply.

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1 If a +/-5 volt supply, or a 10 volt supply, is available, it
2 may not be necessary to provide a tap on the inductor.

3 A resistor 48 performs two functions:

4 a) it adds a +5V DC bias to the RF signal which enables a
5 bias current to be derived for the microphone as more fully
6 described below, and

7 b) it increases the effective damping to control the ring-
8 ing of the transmitter circuit.

9 The effectiveness of diode 35 and transistor 36 on
10 damping is reduced due to inductor 40 being tapped. When
11 data is encoded as the number of cycles in a burst, exces-
12 sive ringing can cause errors.

13 Cable 43 should have a capacitance of approxi-
14 mately 120 pF (typically +/- 40 pF) as measured from one
15 conductor to the other two conductors connected together.
16 It is desirable that cable capacitance represents only a
17 small proportion of the total tuning capacitance. This must
18 be controlled within the stated range, as it forms part of
19 the tuning capacitance for transmitter coil 46.

20 Cable 43 is preferably approximately 80 cm long to
21 suit most individuals, and to allow the speech processor to
22 be worn on a belt while the microphone is at ear level. It
23 may be necessary to adjust the value of capacitor 45 to
24 compensate for changes in capacitance when shorter or longer
25 cables are used.

26 The resistance of each conductor of cable 43
27 should be as low as practical and typically less than two
28 ohms. Losses become significant for lengths in excess of
29 1.5 meters, due to the non-ideal nature of the cable.

30 The voltage at point A consists of a radio fre-
31 quency component and a bias voltage. It is a symmetrical
32 sinusoidal signal with a 5 volt DC offset. The DC bias
33 passes through coil 46 and is smoothed by the combined
34 effect of resistor 48, a capacitor 50, a resistor 52, and an
35 additional capacitor 54. The microphone 56, which is pre-
36 ferably a sensitive electret device of the type used in

1 hearing aids, requires a bias voltage of between 0.9 and 20
2 volts and draws between 25 and 50 microamperes. If another
3 type of microphone is used, it may be necessary to adjust
4 the values of resistor 48 and resistor 52.

5 The power supply rejection of the microphone is
6 quite low (on the order of approximately 5:1). The bias
7 voltage noise must therefore be reduced to less than 10
8 microvolts RMS across the audio band, in order to achieve an
9 acceptable input noise level. It is also necessary to pre-
10 vent injection of RF energy into the microphone output,
11 since this could be demodulated and appear as audio noise.

12 A capacitor 58, an inductor 60 and a capacitor 62
13 form a pi filter network which prevents RF injection to the
14 output terminal of the microphone. An identical pi filter
15 network including a capacitor 64, an inductor 66, and a
16 capacitor 68 is used at the other end of cable 43 to prevent
17 RF injection into the audio signal processing circuit 10A'.
18 In this way, the relatively high level of RF signal coupled
19 onto the audio line of the three-wire cable is attenuated to
20 an insignificant level at the microphone and at the input of
21 the processing circuit.

22 Electret microphone 56 has an output impedance of
23 approximately 3000 ohms. Therefore the total capacitive
24 loading must be limited to avoid degradation of the high
25 frequency response of the microphone. Only frequencies of
26 up to 6 KHz are of interest.

27 The effect of inductors 60 and 66 can be ignored
28 at audio frequencies. If the cable capacitance is approxi-
29 mately 100 pF, the total capacitance of the cable and
30 capacitors 58, 62, 64 and 68 is approximately 2.82 nF, which
31 reduces the audio output of the microphone by less than
32 2.5 dB at 6 KHz.

33 Inductors 60 and 66 are chosen to be the highest
34 value available in miniature chip inductors with the addi-
35 tional constraint that the self resonant frequency is above
36 2.5 MHz. The impedance of inductors 60 and 66 at 2.5 MHz is

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1 7.38 Kohms. The impedance of a 680 pF capacitor at 2.5 MHz
2 is 93.7 ohms.

3 The radio frequency voltage coupled onto the audio
4 line of three wire cable 43 is minimized by the low impe-
5 dance of the parallel combination of capacitors 58 and 62
6 and the capacitance between ground wire 70 and audio signal
7 wire 72, when compared to the inter-cable capacitance to RF
8 line 74. The residual RF voltage is then attenuated both
9 into the microphone by inductor 60 and capacitor 62, and
10 into the speech processing circuit 10A by inductor 66 and
11 capacitor 64, by a total of approximately 38 dB.

12 Typical values for the components used in the
13 schematic diagram of FIG. 4 are:

14	Capacitor 38	68 pf
15	Capacitor 42	56 pf
16	Capacitor 45	680 pf
17	Capacitor 50	0.1 uf
18	Capacitor 54	6.8 uf
19	Capacitors 58, 62, 64 and 68	680 pf
20	Inductors 60 and 66	470 uH
21	Resistor 48	4.7 Kohms
22	Resistor 52	4.7 Kohms

23 The RF signal at point A drives the transmitter
24 resonant circuit including capacitor 45 and inductor 46.
25 Capacitor 50 has a low impedance at 2.5 MHz and thus pro-
26 vides a ground return for the transmitter resonant circuit.
27 Series coupling capacitor 42 couples the output of the
28 class-E stage to the parallel tuned transmitter coil 46.
29 When transmitter coil 46 is uncoupled from a receiver coil
30 80, which is electrically connected to an electronics package
31 82 associated with a cochlear implant under the skin 84 of a
32 patient, the parallel tuned circuit presents a high impe-
33 dance in series with capacitor 42, thus minimizing the de-
34 tuning effect on the class-E stage. While a complex re-
35 lationship may be derived for determining the optimum choice
36 of values for capacitor 38 and capacitor 42, as a practical

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1 matter, capacitor 38 is tuned for minimum transmitter power
2 at maximum coupling (i.e., minimum range) and the value of
3 capacitor 42 is selected to provide sufficient power
4 transfer at minimum coupling (i.e., maximum range). This
5 means that the class-E circuit is optimally tuned, i.e.
6 operating most efficiently, when the load reflected across
7 the transmitter circuit is a maximum. As the reflected
8 impedance increases, the voltage developed across the trans-
9 mitter coil increases, thus compensating for the decreasing
10 coupling coefficient and resulting in a more constant
11 voltage being maintained at the receiver as illustrated in
12 FIG. 5. This is an ideal power versus operating distance
13 characteristic whereby the transmitter power is reduced as
14 the receiver becomes more closely coupled.

15 It will be recognized that the coupling between
16 the transmitter and receiver coils may be reduced not only
17 by increasing the distance therebetween, but also by axial
18 misalignment of the coils. Thus, "maximum range" may occur
19 due to a greater distance between the coils or to misalign-
20 ment. "Minimum range" occurs when the coils are coaxially
21 aligned and at the closest possible distance apart. The
22 distance is determined by the depth of the receiving coil
23 below the skin, skin thickness, and headset design. For
24 the latter, this is the distance between the plane of the
25 transmitter coil and the skin.

26 Although the invention has been described with
27 respect to particular embodiments, it is to be understood
28 that these embodiments are merely illustrative of the
29 application of the principles of the invention. Numerous
30 modifications may be made therein and other arrangements may
31 be devised without departing from the spirit and scope of
32 the invention.

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CLAIMS

What is claimed is:

1. A transmission system for transmitting audio and radio frequency energy comprising:
 - a) a three wire unshielded cable;
 - b) a radio frequency source connected to a first wire and a second wire of said three wire cable;
 - c) an audio frequency source connected to said second wire and a third wire of said three wire cable; and
 - d) filter means coupled to said cable for filtering audio from said audio frequency source to reduce interference from said radio frequency source.
2. The transmission system of claim 1, further comprising means for modulating said radio frequency source, whereby said radio frequency source generates signal components in the audio frequency range.
3. The transmission system of claim 1, wherein radio frequency energy from said radio frequency source is at a voltage level several orders of magnitude higher than voltage of said audio frequency source.
4. The transmission system of claim 1, wherein radio frequency energy from said radio frequency source is at a voltage level of substantially four orders of magnitude higher than voltage of said audio frequency source.
5. The transmission system of claim 1, wherein said filter means is connected to said second wire and said third wire.
6. The transmission system of claim 5, wherein said filter means includes at least one pi network.
7. The transmission system of claim 1, wherein said filter means is coupled to said cable at at least one end thereof.
8. A transmission system for a cochlear implant speech processor comprising:
 - a three wire unshielded cable having a first end and a second end;

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a radio frequency transmitter circuit connected to a first wire and a second wire of said three wire cable at a first end thereof;

a radio frequency transmitter coil coupled to said first wire and said second wire of said three wire cable at the second end thereof;

an audio frequency source coupled to said second wire and a third wire of said three wire cable at said second end;

an audio frequency processing means, for processing audio from said audio frequency source, coupled to said second wire and said third wire at said first end of said cable; and

filter means for filtering said audio so that it is substantially free of energy from said radio frequency transmitter circuit.

9. The transmission system of claim 8, wherein said audio source is a microphone for receiving ambient audio, and said transmitter coil and said microphone are located proximate one another.

10. The transmission system of claim 8, further comprising pulsing means for pulsing said radio frequency transmitter circuit to produce pulsed radio frequency output.

11. The transmission system of claim 8, wherein said filter means includes a filter at at least one end of said cable.

12. The transmission system of claim 11, wherein said filter is a pi network.

13. The transmission system of claim 8, where said filter means is connected to said second wire and said third wire.

14. The transmission system of claim 13, wherein said filter means is a pi network.

15. In a radio frequency transmission system having a transmitter with a first resonant circuit, a

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transmitter coil which is part of a second resonant circuit separate and apart from said first resonant circuit, and coupling means for coupling energy between said first resonant circuit and said second resonant circuit, a method for adjusting the power transferred to a receiving coil comprising the steps of:

- a) placing the transmitter coil at a minimum separation from the receiving coil;
- b) adjusting the resonance in said first resonant circuit so that said transmitter draws minimum power;
- c) separating the transmitter coil and the receiving coil to a maximum separation, and
- d) adjusting said coupling means to couple sufficient energy for reliable transmission to occur at said maximum separation.

16. The method of claim 15, wherein said step of adjusting for resonance in said first resonant circuit comprises adjusting a value of a capacitor.

17. The method of claim 15, wherein said coupling means is a capacitor and said step of adjusting the coupling means comprise changing a value of said capacitor.

18. The method of claim 15, wherein the step of separating said transmitter coil and receiver to a maximum separation, comprises separation to at least one of maximum distance and maximum misalignment.

19. The method of claim 15, wherein said receiver coil is associated with a cochlear implant; said transmitter coil is associated with a cochlear speech processor; and wherein in said step of placing the receiver coil, said minimum separation is defined by placing the transmitter coil coaxially over the receiver coil and at a minimum distance therefrom.

20. A radio frequency transmission system for a cochlear implant comprising

- a transmitter having a first tuned circuit;
- a transmitter coil which is part of a second tuned

- 15 -

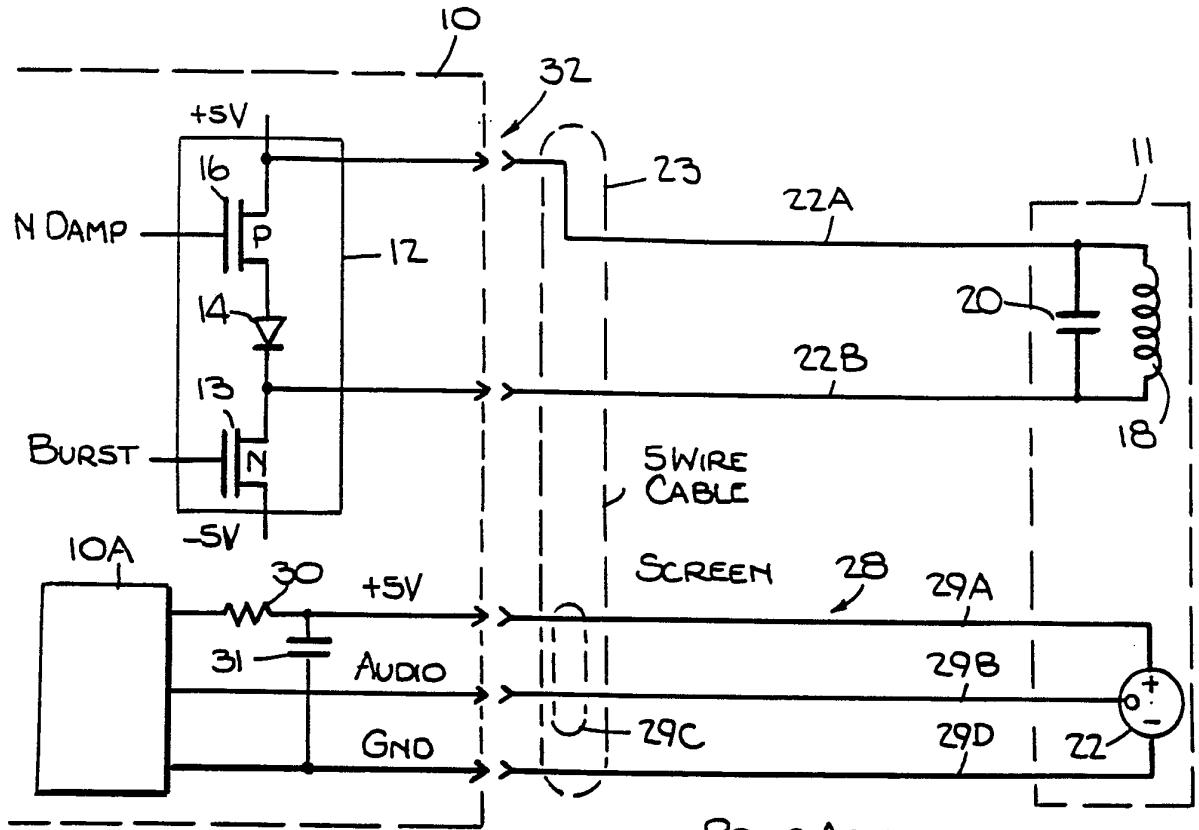
circuit, and

coupling means for coupling radio frequency energy from said first tuned circuit to said second tuned circuit.

21. The radio frequency transmission system of claim 20, further comprising a receiving coil coupled to said transmitter coil; wherein said first tuned circuit has component values adjusted for resonance at a minimum separation between said transmitter coil and said receiving coil, and said coupling means has a value which assures sufficient energy transfer between said transmitter coil and said receiving coil for reliable transmission to occur at a maximum separation.

22. The radio frequency transmission system of claim 20, wherein said coupling means includes a capacitor connected to said first tuned circuit and said second tuned circuit.

23. The radio frequency transmission system of claim 20, wherein said first tuned circuit includes a coil having a tap, said tap and said coil being connected to a radio frequency driver including at least one active device; and wherein said coupling means includes a capacitor, one side of said capacitor being connected to one side of said coil, and the other side of said capacitor being connected to said second tuned circuit.



PRIOR ART
Fig. 1.

Fig. 2A.

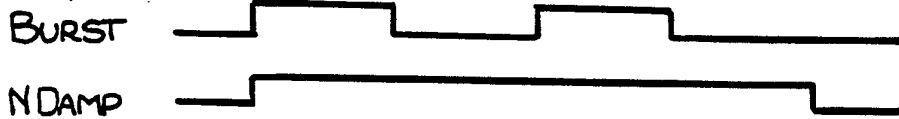
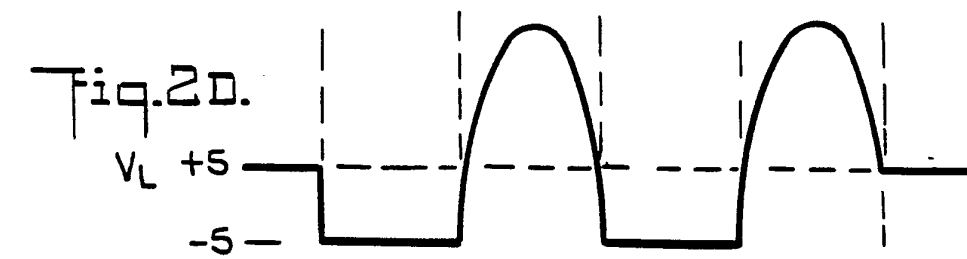


Fig. 2B.



Fig. 2C.



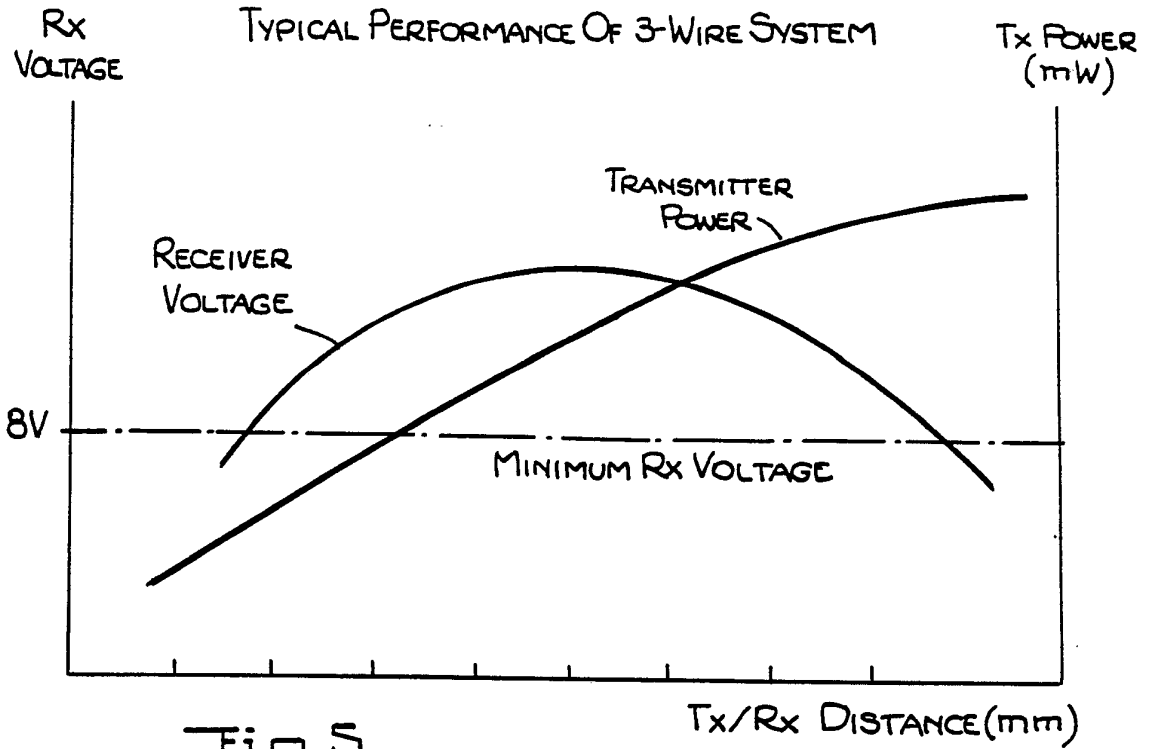
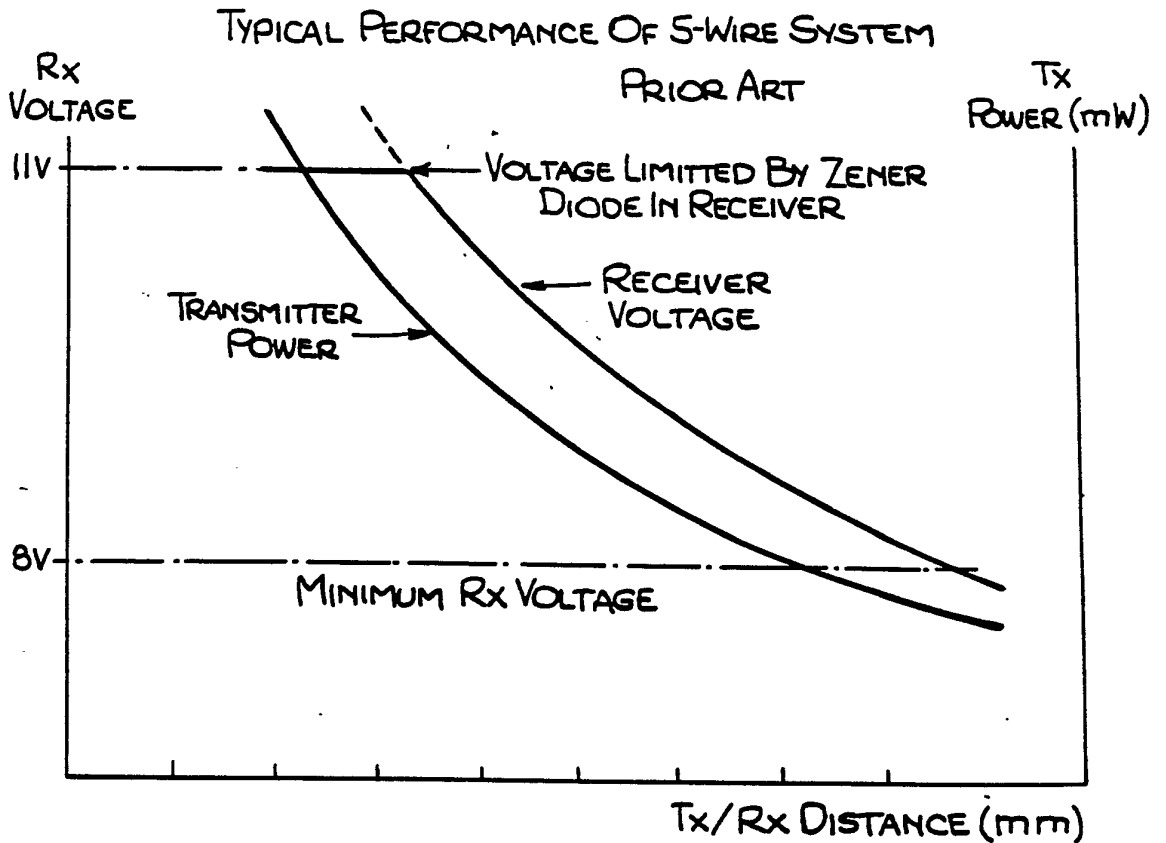


Fig. 5.

Fig. 3.



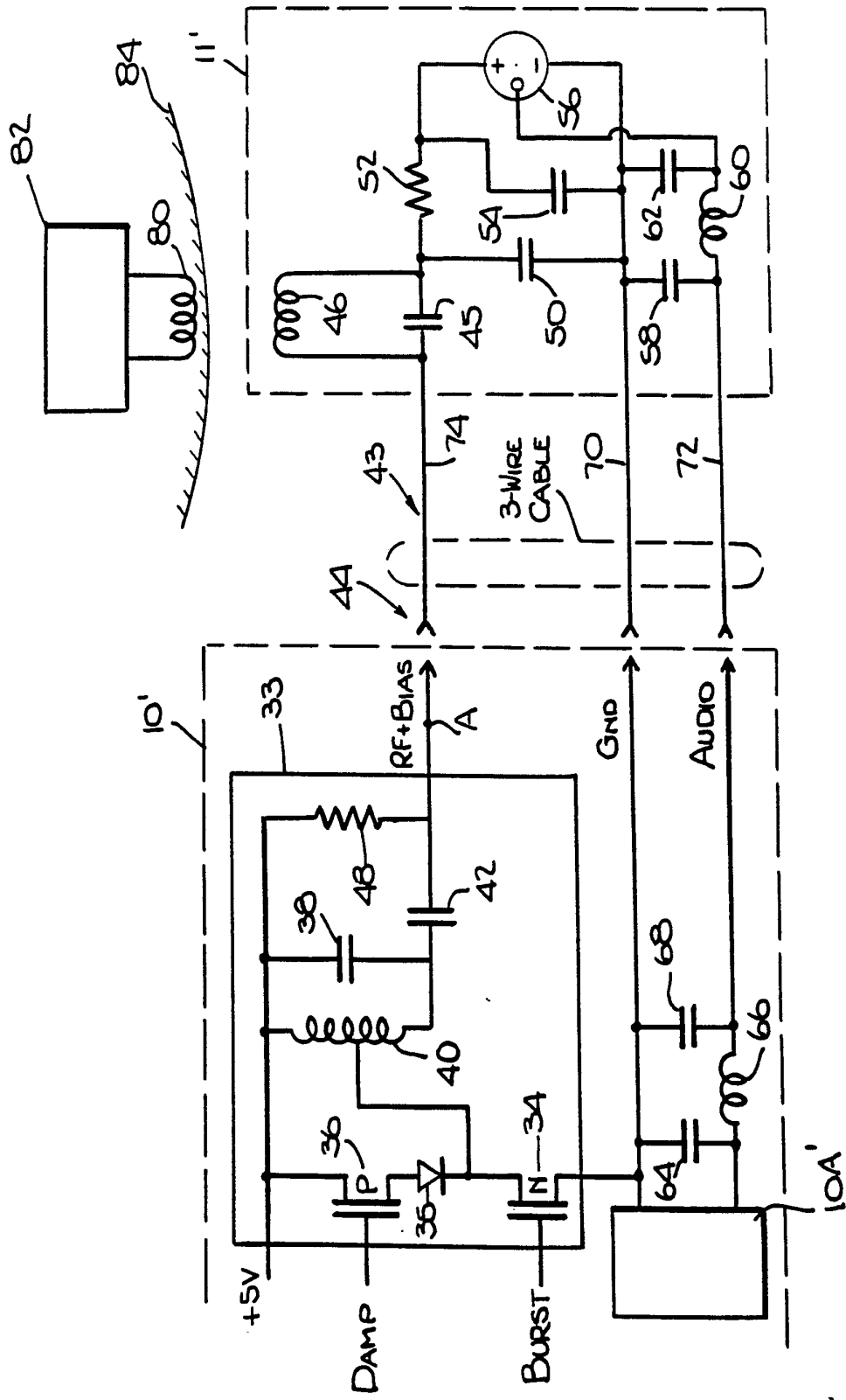


Fig. 4.

INTERNATIONAL SEARCH REPORT

International Application No. **PCT/AU 90/00406**

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all) 6		
According to International Patent Classification (IPC) or to both National Classification and IPC		
Int. Cl. ⁵ H04B 5/00, A61F 11/04		
II. FIELDS SEARCHED		
Minimum Documentation Searched 7		
Classification System	Classification Symbols	
IPC	H04B 5/00, 5/06, 3/32	
Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched 8		
AU: IPC as above, Australian Classification 05.50		
III. DOCUMENTS CONSIDERED TO BE RELEVANT 9		
Category*	Citation of Document, ¹¹ with indication, where appropriate, of the relevant passages 12	Relevant to Claim No 13
Y	Derwent Abstract Accession no. 85-23919/39, Class W01, JP,A, 60-154721 (FUJITSU LTD) 14 August 1985 (14.08.85)	(1-7)
Y	GB,A, 493903 (SIEMENS & HALSKE) 10 November 1938 (10.11.38) See the Figures	(1-7)
Y	DE,A, 1951680 (LICENTIA PATENTVERWALTUNGS GmbH) 22 April 1971 (22.04.71) See the Figures	(1-7)
Y	EP,A, 145430 (MINNESOTA MINING AND MANUFACTURING) 19 June 1985 (19.06.85) See Figures and claim 1	(15-19)
Y	AU,A, 55351/86 (BOARD OF TRUSTEES OF LELAND STANFORD JUNIOR UNIVERSITY) 9 October 1986 (09.10.86) See page 9 line 4 to page 11 line 11	(15-19) (contd)
<p>* Special categories of cited documents: 10 "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"&" document member of the same patent family</p>		
IV. CERTIFICATION		
Date of the Actual Completion of the International Search 26 November 1990 (26.11.90)	Date of Mailing of this International Search Report <i>4 December 1990</i>	
International Searching Authority Australian Patent Office	Signature of Authorized Officer <i>R. Tolhurst</i> R. TOLHURST	

FURTHER INFORMATION CONTINUED FROM THE SECOND SHEET

Y	WO,A, 83/01006 (HOCHMAIR) 31 March 1983 (31.03.83) See Figures, Abstract	(15-19)
Y	The Radio Amateurs Handbook, published 1983, by The American Radio Relay League, see chapter 6 pages 42-43, chapter 7 pages 18-19	(15-19)
A	AU,A, 49009/85 (NUCLEUS LTD and UNIVERSITY OF MELBOURNE) 1 May 1986 (01.05.86)	
A	EP,A, 200231 (HOCHMAIR) 5 November 1986 (05.11.86)	
A,P	US,A, 4918745 (HUTCHISON) 17 April 1990 (17.04.90)	

V. OBSERVATIONS WHERE CERTAIN CLAIMS WERE FOUND UNSEARCHABLE 1

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. Claim numbers ..., because they relate to subject matter not required to be searched by this Authority, namely:

2. Claim numbers , because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. Claim numbers ..., because they are dependent claims and are not drafted in accordance with the second and third sentences of PCT Rule 6.4 (a):

VI. OBSERVATIONS WHERE UNITY OF INVENTION IS LACKING 2

This International Searching Authority found multiple inventions in this international application as follows:

- (1) Transmitting RF and AF over a 3 conductor cable with RF filtering (claims 1-14)
- (2) Adjusting coupling between a Tx coil and a Rx coil (claims 15-19,21)
- (3) A RF transmitter with coupled coils (claims 20,22-23)

1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims of the international application.
2. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims of the international application for which fees were paid, specifically claims:
1-19,21
3. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claim numbers:
4. As all searchable claims could be searched without effort justifying an additional fee, the International Searching Authority did not invite payment of any additional fee.

Remark on Protest

- The additional search fees were accompanied by applicant's protest.
 No protest accompanied the payment of additional search fees.

ANNEX TO THE INTERNATIONAL SEARCH REPORT ON
INTERNATIONAL APPLICATION NO. PCT/AU 90/00406

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report		Patent Family Members			
EP	145430	AU 34910/84 JP 60141034	AU 570741 US 4654880	CA 1226624	
AU	55351/86	CN 86103021 JP 62005358	CN 1005456 US 4679560	EP 200359	
WO	8301006	AT 21216 BR 8207862 DK 1992/83 JP 58501457	AU 89049/82 CA 1192617 DK 156324 US 4441210	AU 551999 DE 3272457 EP 76070	
AU	49009/85	JP 61159972			
EP	200321	AU 54817/86	JP 61276568		

END OF ANNEX