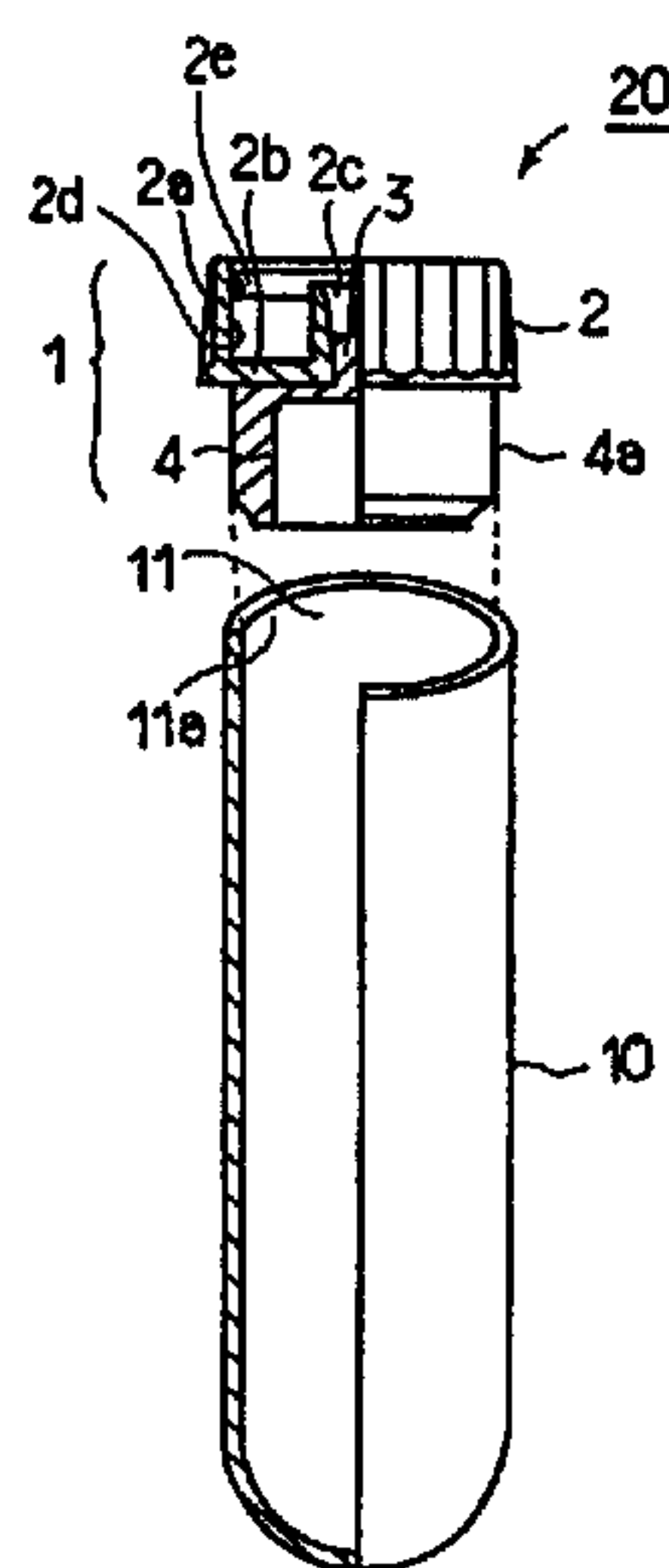


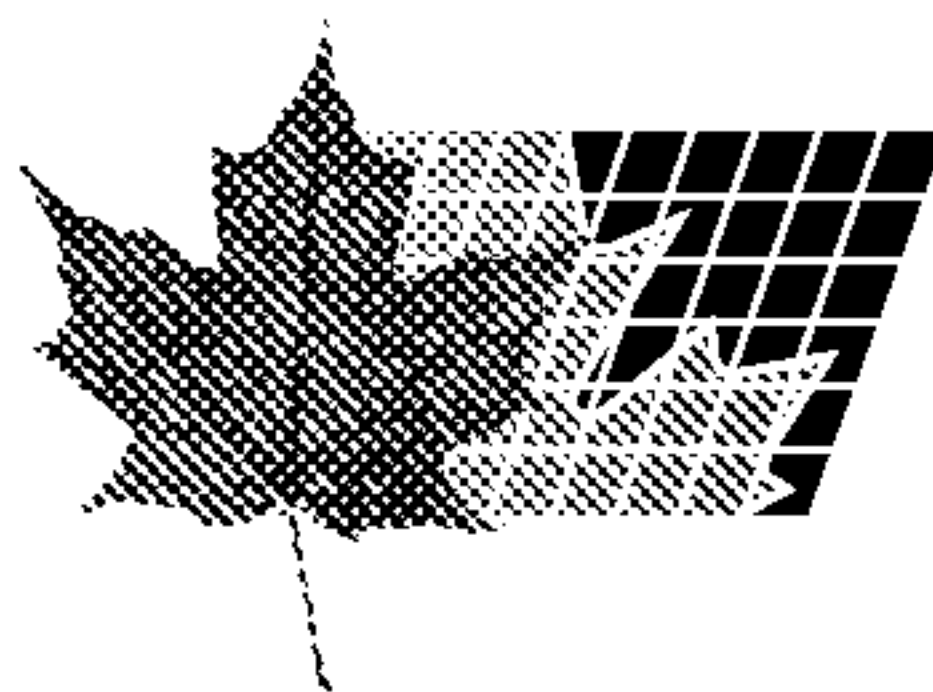


- (72) ANRAKU, HIDEO, JP
(72) OKAMOTO, RYUSUKE, JP
(71) SEKISUI CHEMICAL CO., LTD., JP
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(54) **CORPS DE BOUCHON POUR RECIPIENT DE PRELEVEMENT
D'ECHANTILLONS SOUS VIDE, RECIPIENT DE
PRELEVEMENT D'ECHANTILLONS SOUS VIDE, SYSTEME
DE PRELEVEMENT D'ECHANTILLONS SOUS VIDE,
PORTE-ECHANTILLONS SOUS VIDE, ET COMPOSITION
ELASTOMERE THERMOPLASTIQUE POUR CORPS DE
BOUCHON**
(54) **CLOSURE STRUCTURE FOR VACUUM SPECIMEN
COLLECTION CONTAINER, VACUUM SPECIMEN
COLLECTION CONTAINER, VACUUM SPECIMEN
COLLECTION SYSTEM, HOLDER FOR VACUUM SPECIMEN
COLLECTION SYSTEM AND THERMOPLASTIC
ELASTOMER COMPOSITION FOR FORMING CLOSURE
STRUCTURE**



(57) La présente invention concerne un corps de bouchon (1) pour récipient de prélèvement d'échantillons sous vide, présentant d'excellentes caractéristiques du point de vue de sa productivité, de son aptitude à maintenir le

(57) A plug body (1) for vacuum specimen sampling container excellent in productivity, maintainability of the degree of decompression in a specimen sampling container, needle tube penetrating capability, and needle



degré de décompression dans un récipient de prélèvement d'échantillons, et du point de vue de sa capacité à pénétrer un tube porte-aiguille, ainsi que d'excellentes performances d'obturation d'un trou d'aiguille; ce corps de bouchon étant en outre hermétiquement ajusté de façon amovible dans l'ouverture terminale du récipient de prélèvement d'échantillons, pour que celui-ci puisse être maintenu en décompression. Le corps de bouchon comprend à cet effet une partie (2) de préhension, une partie (3) pénétrant dans le tube porte-aiguille ayant l'élasticité du caoutchouc et placée de façon à obturer le trou (2c) traversant la partie de préhension (2), et une partie (4) raccord élastique caoutchouteuse ajustée hermétiquement dans l'ouverture terminale, en fonction de la forme de la surface interne de l'ouverture terminale du récipient en question. La partie (2) de préhension à une rigidité plus grande que la partie (3) pénétrant dans le tube porte-aiguille et la partie (4) raccord, et une partie (2e) saillante et/ou une partie évidée, destinée à empêcher tout phénomène de recul, est placée sur la surface interne (2d) d'une partie de la paroi latérale annulaire de la partie (2) de préhension.

hole sealing performance and fitted airtight detachably to the opening end of the specimen sampling container so that the specimen sampling container can be maintained under decompressed condition, comprising a holding part (2), a needle tube penetrating part (3) having a rubber elasticity and installed so that it fills up a through-hole (2c) in the holding part (2), and a rubber-like elastic fitting part (4) fitted airtight to an opening end according to the inner surface form of the opening end of the specimen sampling container, the holding part (2) having a rigidity higher than the needle tube penetrating part (3) and the fitting part (4) and at least one projected part (2e) or a recessed part for the prevention of kickback is provided on the internal surface (2d) of an annular side wall part (2a) of the holding part (2).



PCT

特許協力条約に基づいて公開された国際出願

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(21) 国際出願番号 PCT/JP99/01176 (22) 国際出願日 1999年3月10日(10.03.99) (30) 優先権データ 特願平10/68825 1998年3月18日(18.03.98) JP (71) 出願人 (米国を除くすべての指定国について) 積水化学工業株式会社 (SEKISUI CHEMICAL CO., LTD.)(JP/JP) 〒530-8565 大阪府大阪市北区西天満2丁目4番4号 Osaka, (JP) (72) 発明者 ; および (75) 発明者 / 出願人 (米国についてのみ) 安楽秀雄(ANRAKU, Hideo)(JP/JP) 岡本隆介(OKAMOTO, Ryusuke)(JP/JP) 〒746-0006 山口県新南陽市開成町4560 積水化学工業株式会社内 Yamaguchi, (JP) (74) 代理人 弁理士 宮崎主税, 外(MIYAZAKI, Chikara et al.) 〒540-0012 大阪府大阪市中央区谷町1丁目6番5号 西村ビル Osaka, (JP)		(81) 指定国 AU, CA, KR, US, 欧州特許 (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE) 添付公開書類 国際調査報告書
(54)Title: PLUG BODY FOR VACUUM SPECIMEN SAMPLING CONTAINER, VACUUM SPECIMEN SAMPLING CONTAINER, VACUUM SPECIMEN SAMPLING SYSTEM, VACUUM SPECIMEN SAMPLING HOLDER, AND THERMOPLASTIC ELASTOMER COMPOSITION FOR PLUG BODY (54)発明の名称 真空検体採取容器用栓体、真空検体採取容器、真空検体採取システム、真空検体採取ホルダー及び栓体用熱可塑性エラストマー組成物 (57) Abstract A plug body (1) for vacuum specimen sampling container excellent in productivity, maintainability of the degree of decompression in a specimen sampling container, needle tube penetrating capability, and needle hole sealing performance and fitted airtight detachably to the opening end of the specimen sampling container so that the specimen sampling container can be maintained under decompressed condition, comprising a holding part (2), a needle tube penetrating part (3) having a rubber elasticity and installed so that it fills up a through-hole (2c) in the holding part (2), and a rubber-like elastic fitting part (4) fitted airtight to an opening end according to the inner surface form of the opening end of the specimen sampling container, the holding part (2) having a rigidity higher than the needle tube penetrating part (3) and the fitting part (4) and at least one projected part (2e) or a recessed part for the prevention of kickback is provided on the internal surface (2d) of an annular side wall part (2a) of the holding part (2).		

S P E C I F I C A T I O N

CLOSURE STRUCTURE FOR VACUUM SPECIMEN COLLECTION CONTAINER,
VACUUM SPECIMEN COLLECTION CONTAINER, VACUUM SPECIMEN
5 COLLECTION SYSTEM, HOLDER FOR VACUUM SPECIMEN COLLECTION
SYSTEM AND THERMOPLASTIC ELASTOMER COMPOSITION FOR FORMING
CLOSURE STRUCTURE

TECHNICAL FIELD

10 The present invention relates to a closure structure
for a vacuum specimen collection container, a vacuum
specimen collection container incorporating the closure
structure, a vacuum specimen collection system and a holder
for a vacuum specimen collection device, which are employed
15 in conducting analytical tests of liquid specimens such as
blood and urine or gaseous specimens such as expired gas and
working atmosphere, and further to a thermoplastic elastomer
composition for forming the closure structure.

20 BACKGROUND ART

A typical specimen collected by vacuum specimen
collection systems is blood. Accordingly, a vacuum blood
collection container, as illustrative of vacuum specimen
collection containers, is explained below.

25 A typical conventional vacuum blood collection system

is disclosed in Japanese Patent Laying-Open No. 62-227316 (1987). Figure 18 illustrates a basic construction of such a conventional vacuum blood collection system. Figure 18(a) shows a vacuum blood collection tube 30 including a blood
5 collection tube 32 sealed at its open end by attachment of a closure structure 31 having good needle hole sealability and gas barrier properties. Figure 18(b) shows a holder 33 for vacuum blood collection device, into which the vacuum blood collection tube 30 can be inserted. The holder 33 has a
10 blood collection needle retaining bore 34 at its one end. The blood collection needle retaining bore 34 carries an internal thread. Figure 18(c) shows a vacuum blood collection needle 35 which includes a hub 36 having an external thread and needle tips 37, 38 positioned on
15 opposite sides of the hub. The external thread on the hub 36 is configured to screw into the internal thread on the blood collection needle retaining bore 34 of the holder 33 shown in Figure 18(b).

Figure 20 is a perspective view, showing the vacuum
20 blood collection system of Figure 18 while in use for blood collection. When in use for blood collection, the vacuum blood collection needle 35 is screwed into the blood collection needle retaining bore 34. Then, the vacuum blood collection container 30 is inserted in the holder 33 such
25 that the needle tip 37 of the blood collection needle 35 is

forced to penetrate the closure structure 31 to a depth of less than its thickness, whereby the needle tip 37 is kept sealed. This is to prevent the blood from leaking through the needle tip 37 when the needle tip 38 is inserted in a
5 blood vessel.

As shown in Figure 20, an operator holds a whole assembly of blood collection needle 35, holder 33 and blood collection container 30 in an slanted orientation along an axial direction of blood vessel of a subject and then
10 inserts the exposed needle tip 38 in the blood vessel. When the blood collection container 30 is pushed further inside the holder 33, the needle tip 37 is forced to penetrate through the closure structure 31 and the pressure differential between the blood collection container side and
15 the blood vessel side causes the blood to flow into the blood collection container 30. When the pressure differential decreases to zero, the blood ceases to flow. Then, the whole assembly is drawn from the blood vessel to end the blood collection procedure.

20 The above-described blood collection needle 35 is a so-called single blood collection needle for use in introducing blood into a single vacuum blood collection container. In distributing blood into plural vacuum blood collection containers, the needle tip must be kept in a position within
25 the blood vessel while one blood collection container is

replaced by another. Such use of single blood collection needle possibly leads to the leakage of blood from the needle tip 37. Accordingly, a multiple blood collection needle 39 as shown in Figure 19 has come into use. The multiple blood collection needle 39 has an elastic sheath 40 which encloses the needle tip 37 for insertion into the closure structure in an airtight manner to prevent blood leakage therefrom. Where such a multiple blood collection needle 39 is used, the blood collection needle 39 assembled to the holder 33 is operated to penetrate in the blood vessel. Subsequently, the blood collection container 30 is assembled to the holder 33 so that it is brought into communication with the blood vessel. This results in collecting the blood in the blood collection container 30.

Key qualities sought for elastic materials used to form the closure structure 31 as shown in Figure 18(a) include gas barrier properties sufficient to maintain a vacuum pressure within the blood collection container and the ability to seal a needle hole left after the needle tip has been retracted. This has led to the widespread use of crosslinked isobutylene-isoprene rubbers (crosslinked IIR, crosslinked butyl rubber).

The closure structure 31 shown in Figure 18(a) has a configuration most widely adopted in the art. Subsequent to collection of blood, the closure structure 31 is detached to

dispense the blood from the blood collection container 30.

It has been reported, however, that the blood is likely caused to splash the moment the closure structure 31 is detached. This is attributed to the configuration of

5 closure structure adopted to provide the improved seal for better maintaining the interior vacuum pressure of the blood collection container 30. In order to obviate such problems, the use of composite structural closures incorporating a cover disposed to cover a crosslinked butyl rubber closure
10 and prevent splashing of blood has been proposed, for example, by Japanese Patent Laying-Open Nos. Hei 5-168611, Hei 4-215961, Sho 59-228831, Sho 60-242367, Sho 61-170437, Sho 59-230539 and Hei 3-505320.

As stated above, crosslinked butyl rubber has been
15 widely used in the manufacture of closure structures. The use of such crosslinked butyl rubber is however reported to accompany problems, such as the requirements to undergo a prolonged vulcanizing period and subject to washing with water to remove elutable contents thereof, resulting in the
20 reduced productivity.

The crosslinked butyl rubber, because of its inability to be chemically or thermally adhered to a cover member, is physically assembled with the cover member. Such a built-in construction however suffers from a problem of easy
25 separation of the closure structure. For the purpose of

preventing such separation, a construction has been proposed which utilizes a generally double-walled tubular cover member having an inner tubular portion fittingly embedded into the crosslinked butyl rubber member. However, the
5 excellent sealing performance of the crosslinked butyl rubber closure structure relies not only upon the properties intrinsic to the material but also upon the pressure that is exerted on the closure structure when it is fitted in a blood collection tube and acts to close a hole pierced by a
10 needle. Accordingly, the use of the generally double-walled tubular cover member may result in the reduced needle hole sealability.

Japanese Patent Laying-Open No. Sho 57-59536 proposes a closure structure wherein a superior gas barrier film is
15 adhered to or embedded in an inferior gas barrier closure body formed of thermoplastic elastomer. The requirement to add an adhering or embedding process, however, results in sacrificing the high productivity that is a key advantage obtained with the use of thermoplastic elastomer.

20 Closure structures which can be injection molded in a highly productive fashion are disclosed, for example, in Japanese Patent Laying-Open Nos. Sho 58-58057, Sho 61-64253 and Sho 59-28965. These references describe the use of thermoplastic resins and elastomers, as injection moldable
25 materials, which incorporate uncrosslinked butyl rubbers or

flake-form inorganic fillers to assure increased elasticity and gas barrier properties. However, the loading of such additives results in the reduced needle hole sealability, which necessitates incorporation of another thermoplastic elastomer member into a needle cannula pierceable site, and also to the increased resistance to needle penetration.

In Japanese Patent Laying-Open Nos. Hei 4-279152 and Hei 7-51253, a composite structure is proposed. Injection moldable materials, such as thermoplastic elastomer, are used for the needle-pierceable elastic member. The above-described cover for blocking the blood splash is further provided to cover a closure structure. However, no explicit disclosure is not provided as to the improvement in gas barrier properties of thermoplastic elastomers. Simply following a conventional measure, a separate gas barrier sheet is additionally disposed on an upper face of the cover.

In Japanese Patent Laying-Open Nos. Sho 57-154057, Hei 1-76831 and Hei 2-174835 and Utility Model Laying-Open No. Sho 62-160908, sheet-form closures distinct in configuration from typical rubber closures are proposed. A layered sheet such as consisting of an aluminum foil and a needle hole-sealable rubber sheet or rubber tip is directly joined to an open end of a blood collection container by an adhesive or fusion bonding.

This new type of sheet-form closure is reported to have a superior gas barrier property because of its incorporation of a gas impermeable material such as an aluminum foil. It is also reported to exhibit an extremely low resistance to penetration of a blood collection needle, leading to the marked reduction of blood collecting operation load. The high productivity also results. However, the closure once removed from the open end of the blood collection container can not be rejoined thereto. This necessitates separate preparation of a detachable stopper which, when attached, allows storage of specimen in the blood collection container.

Japanese Patent Laying-Open No. Hei 3-97450 proposes a closure formed from injection moldable thermoplastic resins. The closure has an axially-extending communicating hole that permits a needle cannula to pass therethrough. The hole is filled with a needle-pierceable elastic sealing member.

Alternatively, a laminated sealing member consisting of an aluminum foil and a vulcanized rubber sheet is brought into close contact with the hole. The closure is coupled to the blood collection container not by elastic fit commonly adapted for conventional closure structures but by rigid fit between rigid thermoplastic resins. This is reported as being based on the following reason: When the rubber elastic closure is detached from the blood collection tube filled

with blood and then reattached, its superior sealability serves such that an air inside the blood collection tube is prevented from escaping therefrom and is compressed to increase its pressure. The counterforce that the increased
5 pressure exerts against the closure tends to push the closure off the blood collection tube. The use of rigid fit obviates this disadvantage.

The reference describes the rigid fit as being also effective in maintaining an internal vacuum pressure of the
10 blood collection tube. However, molding of thermoplastic resins is often accompanied by defects that disturb close contact of the closure with an inside wall of the blood collection tube or by deformation based on residual strain. Accordingly, the rigid fit used to couple the closure to the
15 blood collection tube presents a problem from an aspect of quality control.

Even in cases where any of the above-described closures is used in combination with the multiple blood collection needle 39 to collect blood, the blood collection container
20 is subjected to a counterforce that the elastic sheath 40 disposed to cover the closure penetrating tip of the blood collection needle exerts when it is compressed. A kickback phenomenon which repels the vacuum blood collection tube from the vacuum blood collection device holder 33 is then
25 likely caused to occur.

In order to prevent the kickback phenomenon, it is required to increase sliding friction resistance either between an outer surface of the closure-penetrating needle cannula 37 and a needle penetrating portion of the closure or between an inner wall surface of the holder and an outer surface of the vacuum blood collection tube. However, the former leads inevitably to the increased resistance to needle penetration. For the latter, it becomes necessary to increase sliding friction resistance or engagement retention between the holder and the blood collection tube or between the holder and the outer surface of the closure, as by providing a ridge or a spring-like elastic tongue on an inner wall surface of the holder or providing a fixed or movable hooking mechanism. However, in either case, the increased resistance results when the blood collection tube is inserted in and pulled out from the holder. This obliges an operator to put the increased strength into its finger tip in a forced posture, leading to the increased tendency for the needle tip to move in the blood vessel. As a result, a heavier burden is imposed on both the operator and subject.

Even in the case where the friction resistance or engagement retention between the holder inner wall surface and the blood collection tube outer surface is increased, outer surface portions of the blood collection tubes or the

closures must be uniformly expanded to diameters which permit slide or engagement thereof with an inner surface of the holder, since one blood collection device holder is usually designed to accommodate various sizes of blood collection tubes and closures. Small-volume blood collection tubes having sizes of about 4 - 7 ml have small diameter tubular bodies. Usually, a test tube rack designed to hold such blood collection tubes define spaces sized for accommodating the tubular bodies at small distances.

Accordingly, the attempt to accommodate the blood collection tubes locally increased in diameter as described above laterally in a row within such a test tube rack fails since the larger diameter portions of those blood collection tubes interfere with each other. This has actually obliged the use of a larger test tube rack designed to accommodate 10 ml tubes, which provides a loose hold to the blood collection tubes and imposes marked inconveniences.

There accordingly remains a need for closure structure for vacuum blood collection container, which can enjoy high productivity and maintain a vacuum pressure within the blood collection tube and which is excellent in needle cannula-pierceable property, needle hole sealability and kickback preventing property.

DISCLOSURE OF THE INVENTION

An object of the present invention is to provide a detachable closure structure for vacuum specimen collection container, which can enjoy high productivity and maintain a vacuum pressure within the blood collection tube and which is excellent in needle cannula-pierceable property, needle hole sealability and kickback preventing property; a vacuum specimen collection container incorporating the closure structure; vacuum specimen collection device holder and a thermoplastic elastomer composition for formation of the closure structure.

A closure structure for a vacuum specimen collection container, in accordance with a first invention of the present invention is constructed such that it can be detachably fitted in an open end of a specimen collection tube in an airtight manner to maintain a vacuum condition inside the specimen collection tube. Characteristically, it includes a grip section having a tubular side wall portion for providing a finger grip, a partition portion extending inward from the side wall portion and a through-hole through which a specimen collection needle cannula can be passed into the specimen collection tube; a rubber-like elastic needle cannula penetrating portion provided to fill up the through-hole in the grip section and having the capability to be pierced by a needle cannula and reseal a hole if left after the needle cannula is retracted; and a rubber-like

elastic fitting portion extending downward from a peripheral edge portion of the rubber-like elastic needle cannula penetrating portion and configured to follow an inner surface profile at the open end of the specimen collection tube so that it can contact fit therein in an airtight fashion. The grip section has a higher rigidity relative to the needle cannula penetrating portion and the fitting portion. Also, the tubular side wall of the grip section is provided on its inner side with at least one raised or recessed portion for kickback preventive purpose.

In a particular aspect of the present invention, the closure structure for a vacuum specimen collection container further includes a fitting portion supporting member which extends from the partition portion toward the fitting portion and is embedded in the fitting portion. This fitting portion supporting member has a lower edge located below a bottom surface of the needle cannula penetrating portion on which a protuberance is provided.

A closure structure for a vacuum specimen collection container, in accordance with a second invention of the present invention, is constructed such that it can be detachably fitted in an open end of a specimen collection tube in an airtight manner to maintain a vacuum condition inside the specimen collection tube. Characteristically, it includes a grip section having a tubular side wall portion

for providing a finger grip, a partition portion extending inward from the side wall portion and a through-hole through which a specimen collection needle cannula can be passed into the specimen collection tube; a rubber-like elastic
5 needle cannula penetrating portion provided to fill up the through-hole in the grip section and having the capability to be pierced by a needle cannula and reseal a hole if left after the needle cannula is retracted; and a rubber-like elastic fitting portion extending downward from a peripheral
10 edge portion of the rubber-like elastic needle cannula penetrating portion and configured to follow an inner surface profile at the open end of the specimen collection tube so that it can contact fit therein in an airtight fashion. In particular, the needle cannula penetrating
15 portion has a protuberance on its bottom surface.

For closure structures for a vacuum specimen collection container according to the first and second inventions of the present application, the through-hole is configured to increase its diameter toward an upward direction from the
20 needle cannula penetrating portion.

In accordance with another particular aspect of the present invention, a wall thickness T_1 (mm) and an oxygen permeability coefficient P_1 ($\text{ml}/\text{cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$) at 25°C of the partition portion in the grip section, a wall thickness
25 T_2 (mm) in a needle penetrating direction and an oxygen

permeability coefficient P2 (ml/cm²·mm⁻¹·sec·cmHg) at 25 °C of the needle cannula penetrating portion, a minimum cross-sectional area Sd (cm²) of the through-hole in the grip section and an open area So (cm²) at the open end of the specimen collection tube are selected to satisfy the following relationship (1):

$$\frac{(S_o - S_d) \times P_1}{T_1} + \frac{S_d \times P_2}{T_2} \leq 10 \times 10^{-10} \quad \dots (1)$$

Preferably, the grip section comprises a thermoplastic resin composition having an oxygen permeability coefficient at 25 °C, P1, of not exceeding 30×10^{-1} ml/cm²·mm⁻¹·sec·cmHg, the needle cannula penetrating portion comprises a thermoplastic elastomer composition having an oxygen permeability coefficient at 25 °C, P2, of not exceeding 700×10^{-1} ml/cm²·mm⁻¹·sec·cmHg, and the fitting portion comprises a thermoplastic elastomer composition having an oxygen permeability coefficient at 25 °C of not exceeding $10,000 \times 10^{-1}$ ml/cm²·mm⁻¹·sec·cmHg. Also, a ratio of a minimum cross-sectional area Sd of the through-hole in the grip section to an open area So at the open end of the specimen collection tube, Sd/So is adjusted not to exceed 0.7.

While not limiting the invention, the grip section is comprised principally of at least one selected from the group consisting of polyester, polyamide, polyallylate,

polyacetal and ethylene-vinyl alcohol copolymer, and the needle penetrating portion and the fitting portion are comprised of thermoplastic elastomer that can be chemically or thermally adhered to the grip section.

5 A vacuum specimen collection container according to the present invention includes a closure structure according to the present invention and a vacuum specimen collection tube.

 In accordance with a particular aspect of the present invention, a vacuum specimen collection container includes a
10 closure structure according to the second invention and a vacuum specimen collection tube having a rubber-like elastic, closure structure receiving portion at an inner face of its open end.

 A vacuum specimen collection system according to the
15 present invention includes a closure structure for a vacuum specimen collection container according to the present invention, a vacuum specimen collection tube, a tubular holder having an opening at its one end for receiving the vacuum specimen collection tube and a means at its another
20 end for retaining a specimen collection needle cannula, and a vacuum specimen collection needle. Provided deep inside the holder on the needle cannula retaining side is an elastic member which has a recessed or raised portion engageable with the raised or recessed portion on the inner
25 side of the tubular side wall in the grip section of the

closure structure.

A holder according to the present invention is the holder for use in combination with a closure structure for a vacuum specimen collection container according to the present invention. The holder is characterized as being tubularly configured to have an opening at its one end for receiving a vacuum specimen collection tube and a means at its another end for retaining a specimen collection needle cannula and as being provided deep inside thereof on the needle cannula retaining side with an elastic member having a recessed or raised portion engageable with the raised or recessed portion on the inner side of the tubular side wall in the grip section of the closure structure.

In accordance with a further aspect of the present invention, a thermoplastic elastomer composition is provided which can be used to form a closure structure for a vacuum specimen collection container according to the present invention. This thermoplastic elastomer composition contains thermoplastic elastomer having rubber elastic domains produced via dynamic crosslinking under a catalyzing action of transition metal oxide, and a compound which can form a water-insoluble salt or chelate with the transition metal.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a partially cut-away sectional view showing a vacuum blood collection container embodiment in accordance with the present invention;

5 Figure 2 is a partially cut-away sectional view showing another closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

10 Figure 3 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

15 Figure 4 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

Figure 5 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

20 Figure 6 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

25 Figure 7 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood

collection container in accordance with the present invention;

Figure 8 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

Figure 9 is a partially cut-away sectional view showing a further closure structure embodiment for a vacuum blood collection container in accordance with the present invention;

Figure 10 is a perspective view showing a blood collection tube embodiment for a vacuum blood collection container in accordance with the present invention;

Figure 11 is a perspective view showing another blood collection tube embodiment for a vacuum blood collection container in accordance with the present invention;

Figure 12 is a partially cut-away sectional view which indicates a size for each part of the closure structure embodiment in accordance with the present invention;

Figure 13(a) and 13(b) are partially cut-away perspective views respectively showing a vacuum blood collection device holder embodiment and another vacuum blood collection device holder in accordance with the present invention;

Figure 14 is a partially-sectioned perspective view

showing another vacuum blood collection container embodiment in accordance with the present invention;

Figure 15 is an exploded perspective view which explains a further vacuum blood collection container
5 embodiment in accordance with the present invention;

Figure 16 (a) is a partially cut-away perspective view which explains a further vacuum blood collection device holder embodiment in accordance with the present invention and 16(b) is a perspective view showing an elastic member
10 incorporated in the holder;

Figure 17 is a partially cut-away sectional view which indicates a size for each part of a conventional closure structure;

Figure 18 is a view showing a basic construction of a
15 conventional blood collection system;

Figure 19 is a side view showing a multiple blood collection needle; and

Figure 20 is a perspective view showing a vacuum blood collection system while in use for blood collection.

20

BEST MODES FOR CARRYING OUT THE INVENTION

The present invention will be now explained with reference to the following embodiments as applied to a vacuum blood collection container for collecting blood.

25 Figure 1 is a partially cut-away sectional view of a

vacuum blood collection container embodiment in accordance with the present invention. A vacuum blood collection container 20 includes a closure structure 1 and a blood collection tube 10. A grip section 2 defines an upper part
5 of the closure structure 1 and is designed to be held by a finger tip when the closure structure is attached to or detached from the blood collection tube. The grip section 2 includes a hollow cylindrical side wall 2a and a partition portion 2b which extends inwardly from a bottom end of the
10 side wall 2a. An inwardly-extending end of the partition portion 2b then projects upward to define a through-hole 2c inside thereof. This through-hole 2c provides a passage through which a blood collection needle cannula can be passed into the blood collection tube 10.

15 For the kickback preventive purpose, an annular rib 2e is provided on an inner surface 2d of the hollow cylindrical side wall 2a to extend circumferentially therealong adjacent its upper edge. The annular rib 2e is disposed such that a plane positioned parallel thereto extends in a direction
20 perpendicular to an axial direction of the closure structure 1, i.e., to an axial direction of the vacuum blood collection tube 20.

The annular rib 2e is designed to engage a springy elastic member 64 which is disposed within an interior
25 portion 63 of a holder 60 for vacuum blood collection

devices, as will be later described with reference to Figure 13, so as to locate on its vacuum blood collection needle holding side. The annular rib 2e resists a rebounding force produced when an elastic sheath 40 on a closure structure penetrating side of the below-described multiple blood collection needle 39 is compressed during blood collection, thereby serving to prevent the occurrence of a kickback phenomenon. When a sufficient pulling force is applied to the blood collection tube 10 on the holder 60 after the blood collection is completed, the annular rib 2e fails to resist the force to finally disengage from a recess 64a.

In this particular embodiment, the annular rib 2e is provided to accomplish the kickback protection. Instead, an annular groove may be provided for the same purpose. In such a case, an engaging part of the elastic member 64 within the interior 63 of the holder 60 is changed in shape to a rib. The groove, alternative to the annular rib 2e or rib 2e, may be provided to extend intermittently, but most preferably continuously around the inner surface 2d of the hollow cylindrical side wall 2a. That is, the kickback preventive rib or groove may be provided locally or in plurality.

A needle cannula penetrating portion 3 is provided to close the through-hole 2c in the grip section 2. This needle cannula penetrating portion 3 is made to exhibit

rubber elasticity and configured to have a larger diameter toward its top end along an axial direction of the closure structure, i.e., constructed in a funnel-like configuration. As will be described later, the through-hole 2c preferably
5 has a minimum cross-sectional area smaller than an open area of an open end 11 of the blood collection tube 10. Thus, the funnel-shaped inner wall around the through-hole 2c serves to precisely guide a vacuum blood collection needle or a sampling nozzle for specimen dispensing into the
10 through-hole 2c.

In the particular embodiment shown in Figure 1, the through-hole 2c is provided concentrically of the closure structure 1, i.e., at a location generally centrally of the grip section 2. However, the through-hole 2c may be shifted
15 in location from a central axis of the closure structure 1. If necessary, the through-hole may be provided in plurality.

The closure structure 1 has a lower fitting portion 4 constructed in a generally hollow cylindrical configuration. The fitting portion 4 is made to exhibit rubber elasticity.
20 Also, the fitting portion 4 is formed to extend downwardly from a peripheral region of a bottom surface of the needle cannula penetrating portion 3. The fitting portion 4 is a part which fits in the open end 11 of the blood collection tube 10 to contact with its inner surface 11a. That is, the
25 fitting portion 4 is designed to fit in the open end 11 of

blood collection tube 10 such that its peripheral surface 4a flexibly follows the surface profile of the inner surface 11a of the open end 11 of blood collection tube 10 to contact therewith. In the present embodiment, the fitting
 5 portion 4 is integrally formed with the needle cannula penetrating portion 3 from the same material.

In the present invention, the particular design parameters are preferably adjusted to satisfy the following relationship (1):

$$\frac{(S_o - S_d) \times P_1}{T_1} + \frac{S_d \times P_2}{T_2} \leq 10 \times 10^{-10} \dots (1)$$

10 where T1 (mm) is a wall thickness of the partition portion 2b of the grip section 2, P1 (ml/cm²·mm⁻¹·sec·cmHg) is an oxygen permeability coefficient of the partition portion at 25 °C, T2 (mm) is a wall thickness of the needle cannula penetrating portion 3 in a needle penetrating direction, P2
 15 (ml/cm²·mm⁻¹·sec·cmHg) is an oxygen permeability coefficient of the needle cannula penetrating portion at 25 °C, Sd (cm²) is a minimum cross-sectional area of the through-hole 2c in the grip section 2, and So (cm²) is an open area at the open end 11 of the blood collection tube 10.

20 The left side of the relationship (1) indicates gas barrier properties of the closure structure 1. If a value X given by the left side of the relationship (1) exceeds 10 x

10⁻¹⁰, the capability of the closure structure to maintain the interior vacuum pressure of the blood collection tube 20 may deteriorate.

5 Examples of materials used to form the grip section 2 include thermoplastic resins, thermosetting resins, metals, ceramics and the like. The use of thermoplastic resins is preferred for its increased productivity and economical efficiency.

10 Examples of materials used to form the needle cannula penetrating portion 3 and the fitting portion 4 include thermoplastic elastomers and thermosetting elastomers. In view of productivity and economical efficiency, the use of thermoplastic elastomers is preferred.

15 More preferably, the closure structure in accordance with the present embodiment satisfies not only the above relationship (1) but also the following conditions:

① The grip section 2 is formed from a thermoplastic resin composition having an oxygen permeability coefficient at 25 °C of not exceeding $30 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$;

20 ② The needle cannula penetrating portion 3 is formed from a thermoplastic elastomer composition having an oxygen permeability coefficient at 25 °C of not exceeding $700 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$;

25 ③ The fitting portion 4 is formed from a thermoplastic elastomer composition having an oxygen permeability

coefficient at 25 °C of not exceeding $10,000 \times 10^{-10}$
ml/cm²·mm⁻¹·sec·cmHg; and

④ The ratio of a minimum cross-sectional area S_d of the
through-hole 2c in the grip section 2 to an open area S_o at
5 the open end 11 of blood collection tube 10, i.e., S_d/S_o
does not exceed 0.7.

As described above, the grip section 2 is preferably
formed from a thermoplastic resin composition having an
oxygen permeability coefficient at 25 °C of not exceeding 30
10 $\times 10^{-10}$ ml/cm²·mm⁻¹·sec·cmHg. Examples of substances which
can be used as a principal constituent of the thermoplastic
resin composition include polyester, polyacrylonitrile,
polyamide, polyallylate, polyacetal, polyacrylate,
polycarbonate, polyvinyl chloride, polyvinylidene chloride,
15 acrylonitrile/styrene copolymer, ethylene/vinyl alcohol
copolymer, polystyrene, polypropylene, high-density
polyethylene, low-density polyethylene and the like. These
substances may be used alone or in any combination thereof.
In the case where two or more of those thermoplastic resins
20 are used in combination, they may be either multilayered or
mixed together.

More preferably, the grip section 2 has an oxygen
permeability coefficient at 25 °C of not exceeding 15×10^{-10}
ml/cm²·mm⁻¹·sec·cmHg. Examples of thermoplastic resins which
25 can impart such an oxygen permeability coefficient to the

grip section include polyester, polyacrylonitrile, poly-
amide, polyallylate, polyacetal, ethylene/vinyl alcohol
copolymer, polyvinyl chloride, polyvinylidene chloride,
polyacrylate, acrylonitrile/styrene copolymer, high-density
5 polyethylene, polycarbonate and the like. These may be used
alone or in any combination thereof.

Still more preferably, the grip section 2 has an oxygen
permeability coefficient at 25 °C of not exceeding 5×10^{-10}
 $\text{ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$. Examples of thermoplastic resins which
10 can impart such an oxygen permeability coefficient to the
grip section include polyester, polyacrylonitrile, poly-
amide, polyallylate, polyacetal, ethylene/vinyl alcohol
copolymer, polyvinyl chloride, polyvinylidene chloride,
polyacrylate, acrylonitrile/styrene copolymer, high-density
15 polyethylene and the like. These may be used alone or in
any combination thereof.

If the oxygen permeability coefficient at 25 °C of the
grip section 2 is excessively high, it may become necessary
to increase a wall thickness of the partition portion 2b in
20 the grip section 2 and/or a wall thickness of the needle
cannula penetrating portion 3. Alternatively, substances
used to form the needle cannula penetrating portion 3 and/or
fitting portion 4 may be limited to those having lower
oxygen permeability coefficients. These possibly result in
25 the increased resistance to needle cannula penetration and

the reduced productivity and economical efficiency.

As stated above, the needle cannula penetrating portion 3 is preferably formed from a thermoplastic elastomer composition having an oxygen permeability coefficient at 25 °C of not exceeding $700 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$. Examples of substances which can be used as a principal constituent of the thermoplastic elastomer composition to impart such an oxygen permeability coefficient thereto include diblock copolymer and triblock copolymer of styrene-, urethane-, amido-, ester-, vinyl chloride- or olefin-based elastomer; and ethylene/vinyl acetate copolymer. These substances may be used alone or in any combination thereof. A variety of additives may further be added to the thermoplastic elastomer composition. In the case where two or more of those thermoplastic elastomers are used in combination, they may be combined in any fashion, e.g., either multilayered or mixed together.

In the case where the olefin-based elastomer is used in combination with the other substance-based elastomers, an additional thermoplastic elastomer may further be used, examples of which include styrene/hydrogenated butadiene block copolymer, styrene/hydrogenated isoprene block copolymer, styrene/isobutylene block copolymer, styrene/ethylene propylene block copolymer and the like.

Where the styrene/hydrogenated butadiene thermoplastic

elastomer is used, the butadiene block preferably contains 1, 2-coupling constituents. Where the styrene/hydrogenated isoprene thermoplastic elastomer is used, the isoprene block preferably contains 3, 4-coupling constituents. The use of
5 the above-described thermoplastic elastomers increases the compatibility of the olefin-based elastomer with other substance-based elastomers.

More preferably, the needle cannula penetrating portion 3 has an oxygen permeability coefficient at 25 °C of not
10 exceeding $200 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$. Examples of substances which can be used as a principal constituent of the thermoplastic elastomer composition to impart such an oxygen permeability coefficient thereto include styrene-based elastomers containing isobutylene blocks, olefin-based
15 elastomers having crosslinked isobutylene domains, urethane-, amido- and ester-based elastomers. These elastomers may be used alone or in any combination thereof.

The crosslinked isobutylene domains having rubber elasticity may be obtained by crosslinking the isobutylene-
20 isoprene copolymer according to a so-called dynamic crosslinking technique. In such a case, transition metal oxides, such as zinc oxide, are frequently used to catalyze the crosslinking reaction. In order to prevent metal ions from eluting from these metal oxide catalysts, it is
25 desirable to use, in combination therewith, compounds that

can react with the metal ions to form insoluble salts or insoluble chelates.

If the oxygen permeability coefficient at 25 °C of the needle cannula penetrating portion 3 is excessively high, it
5 may become necessary to increase a wall thickness of the partition portion 2b in the grip section 2 and/or a wall thickness of the needle cannula penetrating portion 3. Alternatively, substances used to form the grip section 2 may be limited to those having lower oxygen permeability
10 coefficients. These possibly result in the increased resistance to needle cannula penetration and the reduced productivity and economical efficiency.

The above-described thermoplastic elastomers for use in the formation of needle cannula penetrating portion 3 can
15 also be used to form the fitting portion 4. Those comprised primarily of silicone elastomer can also be used. Such elastomers can be used alone or in any combination thereof.

The capability of the needle cannula penetrating portion 3 to provide an airtight seal relies largely upon
20 the magnitude of the oxygen permeability coefficient of the particular rubber elastic material used. In contrast, the ability of the fitting portion 4 to achieve an airtight engagement relies largely upon the flexibility of its peripheral surface 4a to follow the surface profile of the
25 inner surface 11a at the open end 11 of blood collection

tube 10. Accordingly, the oxygen permeability coefficient of the rubber elastic material used to form the vicinity of the peripheral surface 4a may be made larger than that of the needle cannula penetrating portion 3.

5 It is desired that the fitting portion 4 has an oxygen permeability coefficient at 25 °C of not exceeding $10,000 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$. If the oxygen permeability coefficient exceeds the above-specified range, it may become
10 necessary to increase a wall thickness of the partition portion 2b in the grip section 2 and/or a wall thickness of the needle cannula penetrating portion 3. Alternatively, resins used to form the grip section 2 may be limited to those having lower oxygen permeability coefficients. These
15 possibly result in the increased resistance to needle cannula penetration and the reduced productivity and economical efficiency.

 The needle cannula penetrating portion 3 and fitting portion 4 are preferably formed from a thermoplastic elastomer composition having an oxygen permeability
20 coefficient at 25 °C of not exceeding $700 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$, more preferably from a thermoplastic elastomer composition having an oxygen permeability coefficient at 25 °C of not exceeding $200 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$. Still
25 more preferably, the cannula penetrating portion 3 and fitting portion 4 are integrally formed from the same

thermoplastic elastomer composition. This results in the increased productivity.

Also, the outer surface 4a of the fitting portion 4 that is brought into a slidable contact with the inner surface 11a at the open end 11 of blood collection tube 10 preferably has a JIS hardness A or an ASTM Shore hardness A of not exceeding 80, more preferably of not exceeding 60. The excessively high JIS hardness A or ASTM Shore hardness A may lead not only to the increased resistance to needle cannula penetration and fitting into the blood collection tube but also to the looser contact of the fitting portion with the inner surface 11a of the blood collection tube 10, possibly resulting in the reduced working and airtight properties.

Preferably, lubricants, e.g., oils, waxes, aliphatic acids, surfactants, plasticizers and lubricating inorganic fine powders, may be coated onto the outer periphery 4a of the fitting portion 4 by conventionally known techniques such as spraying, dipping and tumbling to facilitate its attachment to or detachment from the open end 11 of the blood collection tube 10. Alternatively, they may be added to the elastomer composition prior to its fabrication into the fitting portion 4.

The ratio, S_d/S_o , of a minimum cross-sectional area S_d of the through-hole 2c in the grip section 2 to an open area

So at the open end 11 of the blood collection tube 10 is preferably designed not to exceed 0.7. If S_d/S_o exceeds 0.7, it may become necessary to increase a wall thickness of the needle cannula penetrating portion 3 and/or a wall
5 thickness of the partition portion 2b in the grip section 2. Alternatively, the materials usable to form the closure structure may be limited to those having lower oxygen permeability coefficients. These possibly result in the increased resistance to needle cannula penetration and the
10 reduced productivity and economical efficiency.

More preferably, S_d/S_o is designed not to exceed 0.5. This allows the reduced wall thickness of the needle cannula penetrating portion 3 or the partition portion 2b in the grip section 2, resulting in the reduced resistance to
15 needle cannula penetration and the increased productivity and economical efficiency. Still more preferably, S_d/S_o is designed not to exceed 0.3. This not only provides the above benefits but also allows the use of closure structure forming materials having relatively large oxygen
20 permeability coefficients, resulting in the further increased economical efficiency.

The grip section 2 is preferably formed from a thermoplastic resin composition comprised principally of at least one non-olefin thermoplastic resin selected from
25 polyester, polyamide, polyallylate, polyacetal and

ethylene/vinyl alcohol copolymer. The needle cannula penetrating portion 3 and fitting portion 4 are preferably formed from a thermoplastic elastomer composition comprised principally of thermoplastic elastomer having the property to be chemically or thermally adhered to the grip section 2. Examples of such principal thermoplastic elastomers include styrene-based elastomers containing isobutylene blocks, olefin-based elastomers having crosslinked isobutylene domains, urethane-, amido- and ester-based elastomers. These elastomers can be used alone or in any combination thereof.

The use of the aforementioned non-olefin thermoplastic resin composition and thermoplastic elastomer composition as forming materials is effective in suppressing the production of toxic gases when they are burned up.

Preferably, the loading of nonflammable fillers in these compositions may be controlled not to exceed 10 wt.%. This results in the reduction in amount of ashes left after the compositions have been burned.

The ability of the needle cannula penetrating portion 3 and fitting portion 4 to be chemically or thermally adhered to the grip section 2 leads to regulating a flow of external atmosphere through between faces of these members, thereby effectively maintaining an interior vacuum pressure of a blood collection container.

The closure structure 1 can be manufactured by a variety of conventionally-known fabrication techniques, such as injection molding, vacuum forming and extrusion. For example, the grip portion 2 is preformed by an injection molding technique and then an insert molding technique is utilized to integrate it with the needle cannula penetrating portion 3 and fitting portion 4. They may be simultaneously formed by a multi-member injection molding technique (multiple injection molding technique). Alternatively, they may be formed separately and then assembled. It is then desired that the separately-formed members are assembled in an airtight manner such that the interior vacuum pressure of the blood collection container can be maintained. To this end, such separate members may be brought into close engagement with each other. More preferably, they may be adhesively joined as by a hotmelt or cure-reactive adhesive, or thermally jointed by a supersonic or high-frequency technique.

Where the constituent members of the closure structure 1 are formed from dissimilar materials, an adhesion promoter or a compatibilizer may preferably be coated or layered on each member to increase their chemical or thermal adhesion. Such additives may alternatively be incorporated in the materials prior to formation into those members.

When desired to facilitate distinguishing the type of a

reagent contained in the blood collection tube 10, the grip section 2 and other constituent members of closure structure 1 may be made discernable by coloring with pigments or dyes, applying prints, or fitting a separately-formed colored member thereto.

The material type of the blood collection tube 10 is not particularly specified, and may be soft glass, hard glass, borosilicate glass or the like. Also useful are rigid thermoplastic resins including polyethylene terephthalate, polybutylene terephthalate, polyethylene naphthalate, polyacrylonitrile, polyamide, polyallylate, polyacrylate, polyvinyl chloride, polyvinylidene chloride, polypropylene, acrylonitrile/styrene copolymer, ethylene/vinyl alcohol copolymer and the like. Particularly suitable is a thermoplastic resin composition containing at least one of the above-listed thermoplastic resins such that it has an oxygen permeability coefficient at 25 °C of not exceeding 30×10^{-10} ml/cm²·mm⁻¹·sec·cmHg. The above-listed thermoplastic resins may be used alone or in combination. In the latter case, two or more of those thermoplastic resins can be used in a layered or kneaded form.

Also, the blood collection tube 10 can be manufactured by a variety of conventionally known techniques, such as injection molding and blow molding. For example, a suitable composition may be extruded into a pipe form and cut to a

desired length. The closure of one end of the pipe, as by attaching a separate member or fitting the closure structure 1 thereto, then results in the formation of a closed-bottom container.

5 The blood collection tube 10 may or may not contain conventionally known reagents and auxiliaries. Examples of reagents include blood coagulation promoter, anticoagulants, glycolysis inhibitors, protease inhibitors, deproteinizing agents, culture media, pH control agents and the like.

10 Examples of auxiliaries include those which serve to help the specimen pretreatment to proceed smoothly, such as serum-separating media, blood component anti-adhesion agents and the like.

 Figure 2 is a partially cut-away sectional view, showing a closure structure for blood collection container in accordance with another embodiment of the present invention. In the closure structure shown in Figure 2, a surface layer portion 4b, which defines at least a part of the peripheral surface 4a of the fitting portion 4 that comes into close contact with the inner surface of the open end of blood collection tube, is constructed from rubber-like material different in type from the needle cannula penetrating portion. As stated earlier, the ability of the needle cannula penetrating portion 3 to provide an airtight

25 closure relies largely upon the magnitude of the oxygen

permeability coefficient of the particular rubber elastic material used. In contrast, the ability of the fitting portion 4 to achieve an airtight engagement relies largely upon the flexibility of its peripheral surface 4a to follow the surface profile of the inner surface 11a at the open end 11 of blood collection tube 10. Accordingly, the oxygen permeability coefficient of the rubber elastic material used to form the vicinity of the peripheral surface 4a may be made larger than that of the needle cannula penetrating portion 3.

Figure 3 is a partially cut-away sectional view, showing a closure structure for blood collection container in accordance with another preferred embodiment of the present invention. In the embodiment shown in Figure 3, a lower portion of the generally hollow cylindrical fitting portion 4 is partially cut out to provide a channel 5 which extends upward from a bottom end of the fitting portion 4. Otherwise, the closure structure is similar in construction to the embodiment shown in Figure 1. Accordingly, the description of other components is omitted here. When the closure structure 1 is attached to or detached from the open end of blood collection tube, the channel 5 allows a gas flow into or from the interior of the blood collection tube. Usually, the closure structure is detached from the blood collection tube for dispensing a part of specimen therefrom.

When it is reattached, an excess open air is entrained and compressed in the interior of the blood collection tube and the compressed air produces a counterforce which acts to push up the closure structure. However, the presence of the
5 channel 5 suppresses the action of such a counterforce to thereby prevent the closure structure from being pushed off by the compressed air.

The shape of the cutout channel 5 is not particularly specified. Preferably, the channel 5 is shaped smoothly so
10 as not to leave sharp edges and capillaries where blood clots could be held to reside.

Figure 4 is a partially cutaway sectional view, showing a closure structure for use in the vacuum blood collection container in accordance with still another embodiment of the
15 present invention. In the embodiment shown in Figure 4, a generally tubular cover 6 is provided to depend from a peripheral bottom edge of the grip section 2 and extend around the generally hollow cylindrical fitting portion 4. The fitting portion 4 is thus located inside the cover 6.
20 The proportion in diameter of the grip section 2 to the fitting portion 4 in this embodiment is made relatively larger compared to those in the embodiments shown in Figures 1 - 3.

The provision of the cover 6, as in the embodiment
25 shown in Figure 4, serves to provide a wider finger grip

region on the closure structure 2, resulting in the improved attaching and detaching operations. The cover 6 length may be dimensioned so that its distal end extends further downward to fully cover the fitting portion 4. Such design
5 shuts off the blood, if caused to splash when the closure structure 1 is detached from the blood collection tube.

Such a cover 6 can be integrally formed with the grip section 2.

Figure 5 is a partially cutaway sectional view, showing
10 a closure structure for use in the vacuum blood collection container in accordance with still another embodiment of the present invention. In this embodiment, the fitting portion 4 is partially cut out to provide the channel 5, as similar to the embodiment shown in Figure 3. The grip section 2 is
15 made relatively larger in diameter and has a peripheral bottom edge from which the cover 6 depends so as to surround the fitting portion 5, as similar to the embodiment shown in Figure 4. This construction not only prevents the closure structure from being caused to move upward when it is
20 detached and then reattached, resulting in the improved attaching and detaching operations, but also shuts off the blood if caused to splash when the closure structure is detached from the blood collection tube.

In the case where both the cutout channel 5 and the
25 cover 6 are provided as illustrated in this embodiment, the

cover 6 is preferably dimensioned so as for its lower end to extend below a deep end of the cutout channel 5. The cover 6 having such a sufficient length can shield the vicinity of the deep end of the cutout channel 5. Accordingly, when the closure structure 1 is detached from the blood collection tube, the cover 6 blocks the blood even if caused to splash through the deep end region of the cutout channel 5 which has just exited from the open end of blood collection tube. This eliminates the possibility for a tester to catch the blood splash.

Where the cutout channel 5 is provided, the blood splashing tends to occur at the deep end region of the cutout channel 5. The cover 6 can thus be made shorter than shown in the embodiment of Figure 4. The relative reduction in length of the cover 6 leads to the reduced area of the cover 6 that shall cover the open end of blood collection tube when the closure structure 1 is attached thereto. This results in the reduced occurrence of the cover 6 to hide a specimen identifying label or a bar code that may be affixed or printed on an outer wall surface of the blood collection tube.

Figure 6 is a partially cutaway sectional view, showing a closure structure for use in the vacuum blood collection container in accordance with still another embodiment of the present invention. In this embodiment, a member 7 is

provided to support the fitting portion. This supporting member 7 extends downward from the partition portion 2b in the grip section 2 into a body of the fitting portion 4. The supporting member 7 has a generally tubular configuration and is embedded into the generally tubular fitting portion 4.

The needle cannula penetrating portion 3 has an inner surface 8 which faces toward the blood collection tube and is positioned to locate above a lower end of the supporting member 7. A generally semi-spherical protuberance 8a is formed on the inner surface 8.

The supporting member 7 is provided to increase the structural integrity of the grip section 2 with the fitting portion 4. Besides, it serves to suppress the excessive deformation of the rubber-like elastic fitting portion 4 when the closure structure 1 is detached or attached.

However, the provision of the supporting member 7 may influence in such a manner as to reduce the stress produced between the fitting portion 4, which acts to reseal a needle hole if pierced in the needle cannula penetrating portion 3, and the open end 11 of blood collection tube 10, possibly resulting in the reduced needle hole resealability.

When the internal pressure of a specimen contained in the blood collection tube 10 is caused to build up for some reason, a hydrostatic pressure applies in a direction normal

to the inner surface 8 of the needle cannula penetrating
portion 3. Because the penetrating direction of the needle
is generally perpendicular to the inner surface 8, the
hydrostatic pressure applies in the penetrating direction of
5 the needle. This may cause a backflow of the specimen to
occur while readily push widening the needle hole, possibly
resulting in the leakage toward an outer surface of the
needle cannula penetrating portion 3.

10 However, since the needle cannula penetrating portion 3
in the present embodiment has the protuberance 8a on its
inner surface 8, the hydrostatic pressure applies not in the
penetrating direction of needle but in a direction normal to
a surface of the protuberance 8a, i.e., in a direction to
close the needle hole. This results in the increased needle
15 hole sealability.

The configuration of the protuberance 8a is not limited
to the general semi-sphere, and may be generally cylindrical
or generally truncated conical. The protuberance 8a is
preferably integrally formed with the needle cannula
20 penetrating portion 3.

While shown in the embedded form, the supporting member
7 may be arranged to extend along the inner wall surface of
the fitting portion 4. Also, while shown to be generally
tubular, the supporting member 7 may consist of pillars
25 circumferentially arranged in a row.

Figure 7 is a partially cutaway sectional view, showing a closure structure for use in the vacuum blood collection container in accordance with still another embodiment of the present invention. In this embodiment, the supporting member 7 for reinforcing the fitting portion 4 is provided in the grip section 2, and the cutout channel 5 in the fitting portion 4, as similar to the embodiment shown in figure 6. The closure structure 1 can thus be prevented from being pushed off by compressed air when the closure structure 1 once detached from the blood collection tube is reattached thereto.

Figure 8 is a partially cutaway sectional view, showing a closure structure for use in the vacuum blood collection container in accordance with still another embodiment of the present invention. In this embodiment, the supporting member 7 is provided to reinforce the fitting portion 4 which is circumferentially surrounded by the cover 6. The provision of the cover 6 results in obtaining the same action and effect as in the embodiment shown in Figure 4. In the fabrication of the grip section 2, the supporting member 7 and cover 6 can be integrally formed.

Figure 9 is a partially cutaway sectional view, showing a closure structure for use in the vacuum blood collection container in accordance with still another embodiment of the present invention. In this embodiment, the supporting

member 7 is provided to reinforce the fitting portion 4 which has the cutout channel 5 and is circumferentially surrounded by the cover 6. The provision of the cutout channel 5 and cover 6 results in obtaining the same action and effect as in the embodiment shown in Figure 5.

Figure 10 is a perspective view of a blood collection tube for use in vacuum blood collection containers in accordance with the above-described embodiments. The shown blood collection tube is identical to that shown in Figure 1. The configuration of the blood collection tube for use in the present invention is not limited to that shown in Figure 10. Various configurations of blood collection tubes, including conventionally known tubes, can be employed which include, for example, the bottle-like blood collection tube having a diameter reduced toward a top opening end and increased toward a bottom end as shown in Figure 11.

Figure 13(a) is a partially cutaway sectional view, showing a holder for vacuum blood collection devices in accordance with still another embodiment of the present invention.

The vacuum blood collection device holder 60 has at its one end an opening 61 which allows insertion of a vacuum blood collection tube 20 thereinto and at its other end a needle holding portion 62 for retaining a vacuum blood collection needle 39. A spring-like elastic member 64 is

disposed at an innermost portion 63 of the holder 60 adjacent the holding portion 62. The spring-like elastic member 64 has a groove 64a which is configured to be freely engageable with the aforementioned kickback-preventive rib 2e of the closure structure 1. The groove 64a of spring-like elastic member 64 is spaced from an inner surface of the innermost portion 63 to extend parallel thereto.

The elastic member 64 may be disposed at one or more locations and preferably at plural locations along a general circle. In the case where the kickback preventive element in the closure structure 1 is changed in configuration from a rib to a groove, the groove 64a in the holder 60 will be accordingly changed to a rib.

Various types of thermoplastic resins, thermosetting resins and metals can be used to form the spring-like elastic member 64. The use of thermoplastic resins is preferred for the increased productivity, although it is not limiting. That is, the use of tough and rigid thermoplastic resins is preferred, examples of which include polyester, polyamide, polyallylate, polyoxymethylene (polyacetal), polycarbonate, polypropylene, acrylonitrile/butadiene/styrene copolymer (acrylonitrile/styrene copolymer) and the like.

The spring-like elastic member 64 may be integrally formed with the holder 60. Alternatively, the separately

formed spring-like elastic member may be joined to the holder 60. The technique to join them is not particularly specified. They may be joined adhesively, thermally or by a mating structure provided between them.

5 The elastic member 64 may be constructed in a generally tubular form such that the groove 64a extends continuously around a peripheral surface of the elastic member, as shown in Figure 13(b). Such a construction increases the rigidity of the elastic member and accordingly allows the formation
10 of elastic member 64, as a separate member, from rubber elastic materials such as thermoplastic elastomers and thermosetting elastomers. The separately formed elastic member 64 will be secured to the innermost portion 63 of the holder 64.

15 When in use, the holder 60 retains a vacuum blood collection needle 39. A needle cannula 38 is then inserted into a blood vessel. Subsequently, the vacuum blood collection tube 20 carrying the closure structure 1 attached thereto is inserted in the holder 60. As the needle cannula
20 37 advances deeper in the needle cannula penetrating portion 3 of the closure structure 1, an elastic sheath 40 is more compressed and a counterforce accompanying the compression starts to be applied to the vacuum blood collection tube 20. However, when an upper end of the tubular side wall 2a in
25 the grip section 2 of the closure structure 1 advances

between the elastic member 64 and the inner surface of the holder and reaches a position where the rib 2e on the closure structure 1 engages with the groove 64a on the holder 64, the engagement withstands the counterforce
5 accompanying compression of the elastic sheath 40 so that the vacuum blood collection tube 20 can be kept retained within the holder 60. This allows the blood collection to proceed smoothly.

When the blood collection is completed, a force may be
10 applied in a pulling direction so that the rib 2e is caused to disengage from the groove 64a, whereby the vacuum blood collection tube 20 can be removed from the holder 60.

As described above, the kickback prevention is achieved by utilizing the inner surface of side wall 2a in the grip
15 section 2 of closure structure 1. This eliminates the need to enlarge an outer diameter of the grip section 2 to such an extent that an outer surface of the grip section 2 can be brought into slidable contact with an inner surface of the holder. Accordingly, even in the case where a small-size
20 vacuum blood collection tube having a volume of 4 - 7 ml is employed, it can be inserted smoothly in a conventional test tube rack and retained in an upright position.

Figure 14 is a partially cut-away fragmentary sectional view, showing a vacuum blood collection tube in accordance
25 with still another embodiment of the present invention. The

vacuum blood collection tube 90 has a closure structure 70 and a blood collection tube 80.

In the closure structure 70, the kickback preventive rib 2e is not formed. The protuberance 8a is provided on a bottom surface 8 of the needle cannula penetrating portion 3. A fitting portion 74 is disposed to extend downward from a bottom surface of a partition portion 72b. Otherwise, the closure structure 70 is similar in construction to the closure structure 1 shown in Figure 1.

Accordingly, the descriptions of like parts are omitted here by denoting them like reference numerals.

In the closure structure 70, the needle cannula penetrating portion 3 is disposed to close the through-hole 2c and is provided at its bottom face 8 with the generally semi-spherical protuberance 8a. The provision of the protuberance 8a increases the needle hole sealability.

In the blood collection tube 80, a bottom-closed tubular container 82 having rubber elasticity fits inside a bottom-closed rigid tubular container 83, like a telescopic structure, whereby the inner face at the opening end of the blood collection tube 80 provides a rubber elastic surface which receives the closure structure. Since the inner surface 80a of the blood collection tube 80 is flexible enough to follow a profile of an outer surface 74a of fitting portion 74, the closure structure 70 can be attached

to the blood collection tube in an airtight fashion and accordingly the interior vacuum pressure of the blood collection tube 80 can be maintained.

5 Instead of using the rubber elastic tubular container 83, a rubber-like elastic material may be provided only on an inner surface region of the tubular container 82 that receives the outer surface 74a of the fitting portion 74.

10 Also in the vacuum blood collection container according to this embodiment, a kickback preventive rib or groove may be formed in the closure structure 70.

The general and preferred materials listed in the preceding description of the vacuum blood collection container 20 shown in Figure 1 can also be used to form a grip section 72 and the needle cannula penetrating portion 3
15 in this embodiment.

The rigid tubular container 82 can be formed from various types of thermoplastic and thermosetting resins. Preferred examples of the material and oxygen permeability coefficient at 25 °C are similar to the case of the blood
20 collection tube 10 for use in the blood collection container shown in Figure 1.

On the other hand, the rubber-like elastic tubular container 83 may be formed from a thermoplastic elastomer composition comprised principally of a thermoplastic
25 elastomer, examples of which include diblock, triblock or

higher-order block copolymers of styrene-, urethane-, amido-, ester-, vinyl chloride- or olefin-based elastomer; and ethylene-vinyl acetate copolymers. These thermoplastic elastomers may be used alone or in any combination thereof.

5 In the case where two or more types of thermoplastic elastomers are used in combination, they may be combined in any form. For example, they may be layered or mixed. Also, various additives may be incorporated in the thermoplastic resin composition.

10 Thermosetting elastomers, such as silicone-based elastomers, may alternatively be used to form the rubber-like elastic tubular container 83.

It is necessary that the rubber-like elastic tubular container 83 be joined, either adhesively or thermally, to the rigid tubular container 82. In such cases, various types of chemical or thermal adhesion modifiers may be applied to an interface therebetween. Preferably, the aforementioned thermoplastic or thermosetting elastomers have intrinsic chemical or thermal adhesion properties.

15 Accordingly, those comprised principally of at least one of urethane-, amido-, ester- and styrene-based thermoplastic elastomers, triblock or higher-order composite copolymers with styrene-based elastomer, either with or without the addition of various additives, are suitably used. The

20 primer-incorporated silicone-based thermosetting elastomer

25

can also be used suitably.

In the manufacture of the blood collection tube 80, the rubber-like elastic tubular container 83 may be inserted in the separately-formed tubular container 82 and then joined
5 together by adhesives or fusion. Conventionally known techniques, such as multiple injection molding, can also be utilized to manufacture the blood collection tube.

The blood collection tube may be manufactured by a technique which involves coextruding the above-described
10 thermoplastic resin and thermoplastic elastomer into a two-layer pipe, cutting the pipe to a desired length, and fitting a sealing member 84 separately formed from the aforementioned thermoplastic resin into one open end of the two-layer pipe, as shown in Figure 15. This technique
15 allows the manufacture of the blood collection tube having an optional length.

Instead of using the sealing member 84, the closure structure 70 may be fittingly attached to the two-layer pipe, as shown on a lower right side of Figure 15, so that a
20 blood collection tube is constructed which allows specimen extraction from both ends.

In the present invention, the preferred thermoplastic elastomer composition includes thermoplastic elastomer having crosslinked rubber elastic domains and contains a
25 compound which form water-insoluble salts or chelates with

transition metals.

The metal oxides often used as catalysts for dynamic crosslinking of the aforementioned rubber elastic domains tend to remain in the elastomer by an excess amount even
5 after termination of the crosslinking reaction. When the closure structure formed from such elastomer is contacted with an aqueous specimen, metal ions in the metal oxides may be caused to dissolve into the specimen.

In order to prevent the metal ions from being dissolved
10 into the specimen, such metal ions may be extracted using dilute hydrochloric acid or the like from the elastomer either before or after it is formed into the closure structure. More preferably, the aforementioned compound that forms water-insoluble salts or chelates with transition
15 metals may be incorporated in the elastomer before it is formed into the closure structure, so that the elution of the metal ions can be effectively suppressed.

Examples of compounds that form water-insoluble salts include higher fatty acids containing a hydrophobic residual
20 group and a carboxylic group, such as naphthenic acid, octylic acid, oleic acid, erucic acid, stearic acid and soybean oil fatty acid; and polymeric compounds containing a carboxylic residual group, such as acrylic acid, methacrylic acid, maleic acid and maleic anhydride.

25 Illustrative of suitable compounds that form water-

insoluble chelates are monomeric and polymeric compounds containing a hydrophobic residual group and O,O ligand, O,N ligand, O,S ligand, N,N ligand, N,S ligand or S,S ligand. Examples of such compounds include monomeric compounds such
5 as diethylenetriamine pentaacetic acid, triethylenetetramine hexaacetic acid, 2-mercaptobenzothiazole, N-benzoyl-N-phenylhydroxylamine, N-cinnamoyl-N-phenylhydroxylamine, o-(salicylidene)thiophenol and the like; and polymeric compounds containing a residual group and an amide linkage
10 such as ethylenediamine tetraacetic acid and porphyrin.

These compounds can be mixed with the aforementioned thermoplastic elastomer after they have been solubilized by a solvent, or by a melt kneading technique using an extrusion kneader. These compounds may be fed into a hopper
15 in a forming machine or a Banbury mixer and stirred for mixture with the thermoplastic elastomer prior to being formed.

These compounds that form water-insoluble salts or chelates may be dispersed in particulate form in the
20 thermoplastic elastomer, but preferably dispersed uniformly throughout the elastomer to promote the formation of salts or chelates with remaining transition metals. More preferably, the compounds used have melting points of not above the fabrication temperature of the elastomer.

25 The thermoplastic elastomer composition in accordance

with the present invention may be used to form a whole element of the closure structure for vacuum specimen collection container, but preferably to form the needle cannula penetrating portion having rubber elasticity and the rubber-like elastic fitting portion, as a minimum, whereby the metal ions are prevented from dissolving into the specimen.

EXAMPLES

10 The present invention will be now described in detail with reference to specific examples.

 The following example uses the closure structure embodiment shown in Figure 9, with the exception that the semi-spherical protuberance 8a is excluded from the bottom surface 8 of the needle cannula penetrating portion 3.

15 Figure 12 is a partially cut-away sectional view which indicates a size for each part of the closure structure shown in Figure 9. In Figure 12, a indicates a minimum diameter of the through-hole 2c, b indicates an outer diameter of the fitting portion 4, c indicates a thickness of the needle cannula penetrating portion 3, d indicates a thickness of the partition portion 2b, e indicates a length of the cutout channel, f indicates a length of the cover 6, g indicates a length of a portion of the fitting portion 4

20 that has a constant outer diameter, h indicates a length of

25

a tapered portion at the top end of the fitting portion 4, i indicates a whole length of the closure structure 1 and j indicates an outer diameter of a bulk of the closure structure 1.

5 1. EXAMPLES AND COMPARATIVE EXAMPLES CONCERNING THE ABILITY OF THE CLOSURE STRUCTURE TO MAINTAIN LOW PRESSURE

EXAMPLES 1 - 19

(Manufacture of a Vacuum Blood Collection Tube)

10 The dimension (unit: mm) of each part of the closure structure of Figure 12, the type and oxygen permeability coefficient (unit: $\text{ml}/\text{cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$) of the material used to form the grip section including the cover and the fitting portion supporting member, the type, Shore hardness A and oxygen permeability coefficient (unit: $\text{ml}/\text{cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$)

15 of the material used to form the needle cannula penetrating portion and fitting portion, for each Examples, are given in Tables 1 - 3. The type of the adhesion modifier used to provide the improved adhesive surfaces, as well as the type of the lubricant used to reduce friction when the closure

20 structure is attached or detached, are also indicated in Tables 2 and 3. The ratio S_d/S_o of the minimum cross-sectional area S_d of the needle cannula penetrating portion to the cross-sectional area S_o at the open end of the blood collection tube, as well as the value calculated from the

25 left side of the relationship (1), are also indicated in

Tables 2 and 3.

In the manufacture of each closure structure, the grip section was injection molded, a small amount of adhesive was optionally applied onto its joint surface and then dried, and subsequently the needle cannula penetrating portion and fitting portion were insert molded. Finally, a small amount of lubricant was coated onto a surface of the fitting portion. Also, a kickback preventive annular rib was formed to extend along an inner peripheral surface of the annular side wall in the grip section.

Polyethylene terephthalate was injection molded into a blood collection tube having an inner diameter at its open end of 10.7 mm, a whole length of 100 mm and a volume of 7 ml. Each closure structure was press fitted in the blood collection tube under a reduced pressure to prepare a vacuum blood collection tube purposed to collect 6 ml blood.

(Evaluation)

Commercially available 21G multiple vacuum blood collection needle and needle holder without a kickback preventing mechanism were utilized to suction collect 30 °C water in each of the above-obtained vacuum blood collection tubes according to a conventional vacuum blood collection procedure. During the suction collection, a bottom portion of the blood collection tube was held by a finger tip to prevent a kickback. The actual weight of the collected

water was calculated from the difference in weight of the blood collection tube before and after introduction of the water by suction. The measurement in weight of the water suction collected was performed twice, immediately after the
5 manufacture of the vacuum blood collection tube and after it was stored in a 50 °C oven for a week, to evaluate the change in capability of the tube to collect the water by suction with the lapse of time after its manufacture. Also, the resistance of the vacuum blood collection needle was
10 evaluated organoleptically. In addition, the vacuum blood collection tube, after collection of water by suction, was held in a reversed orientation for 30 seconds, during which time possible leakage of water droplets through the needle hole was visually observed, to evaluate the needle hole
15 sealability.

COMPARATIVE EXAMPLE 1

(Manufacture of a Vacuum Blood Collection Tube)

Crosslinked butyl rubber was compression molded into a closure structure having an oxygen permeability coefficient
20 of about $30 \times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$ and measuring the dimension (unit: mm) given in Table 2 for each part, which corresponded to those of rubber closures generally available in the market. Their details are given in Table 4. A small amount of polydimethyl siloxane was subsequently coated onto
25 a surface of a fitting portion to reduce friction during the

attachment or detachment of the closure structure. A vacuum blood collection tube purposed to collect 6 ml blood was manufactured using the above-obtained closure structure in the same manner as in Examples 1 - 19.

5 (Evaluation)

The closure structure was evaluated in the same manner as in Examples 1 - 19.

EXAMPLES 20 -22

(Manufacture of a Vacuum Blood Collection Tube)

10 Vacuum blood collection tubes each purposed to collect 5 ml blood and having the specification shown in Table 1 were manufactured in the same manner as in Examples 1 - 19.

(Evaluation)

15 Each closure structure was evaluated in the same manner as in Examples 1 - 19.

(Results of Examples 1 -22 and Comparative Example 1)

20 The results obtained for the above Examples are given in Table 5, collectively. The vacuum blood collection tubes obtained in Examples 1 - 19 provided satisfactory results as comparable to those of the vacuum blood collection tube of Comparative Example 1, in terms of properties such as the capability to maintain a vacuum pressure, resistance to penetration of blood collection needle and needle hole sealability. In contrast, the vacuum blood collection tubes
25 of Examples 20 - 22 show the reduced capability to maintain

a vacuum pressure because of their closure structures which failed to satisfy the relationship (1). However, the vacuum blood collection tubes of Examples 20 - 22 provided satisfactory results as comparable to those of the vacuum
5 blood collection tube of Comparative Example 1, in terms of resistance to penetration of blood collection needle and needle hole sealability.

Table 1

		Size										Grip Section	
		a	b	c	d	e	f	g	h	i	j	Material Type (Thermoplastic Resin)	1)*
Ex.	1	2.4	11	4	2	4	4	5	2	13	17	Polyethylene Terephthalate	1
	2	2.4	11	4	2	4	4	5	2	13	17	Nylon	0.5
	3	2.4	11	4	2	4	4	5	2	13	17	Acrylonitrile-Styrene Copolymer	4
	4	2.8	11	3	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
	5	4.8	11	3	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
	6	7.6	11	3	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
	7	1.9	11	4	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
	8	1.9	11	4	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
	9	1.9	11	4	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
	10	8.5	11	6	2	4	4	5	2	13	17	Polyethylene Terephthalate	1
	11	8.5	11	6	2	4	4	5	2	13	17	Polypropylene	20
	12	4.0	11	3	1	4	4	5	2	13	17	Polyethylene Naphthalate	0.3
	13	4.0	11	3	1	4	4	5	2	13	17	Polybutylene Terephthalate	1
	14	3.0	11	7	0.5	4	4	5	2	13	17	Polyethylene Terephthalate	1
	15	6.0	11	4	1	4	4	5	2	13	17	Polyacrylonitrile	0.1
	16	4.0	11	6	1	4	4	5	2	13	17	Ethylene-Vinyl Alcohol Copolymer	0.05
	17	4.0	11	3	1	4	4	5	2	13	17	Polybutylene Terephthalate	1
	18	4.0	11	3	1	4	4	5	2	13	17	Polybutylene Terephthalate	1
	19	4.0	11	3	1	4	4	5	2	13	17	Polybutylene Terephthalate	1
	20	1.9	11	4	1	4	4	5	2	13	17	Polypropylene	20
	21	3.0	11	4	4	4	4	5	2	13	17	Polypropylene	20
	22	1.9	11	4	1	4	4	5	2	13	17	Polyethylene Terephthalate	1

1)* Approximate Oxygen Permeability Coefficient:

Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

Table 2

	Needle Cannula Penetrating Portion/ Fitting Portion			Adhesion Promoter	Applied Lubricant	Sd/ So	3) *
	Material Type (Thermoplastic Elastmer)	1) *	2) *				
Ex.	1	Styrenic (Rabalon, Prod. of Mitsubishi Chemical)	400	60	Applied, Chemlock481 (Prod. Of Rode Far East)	Polydimethyl Siloxane	0.05 5.5
	2	Styrene- Isobutylene Based (TS Polymer, Prod. of Kuraray)	30	55	Applied, Chemlock481 (Prod. Of Rode Far East)	Polypropylene Glycol	0.05 0.6
	3	Styrene- Crosslinked Isobutylene Based (ITS Polymer, Prod. of Kuraray)	30	60	Applied, Chemlock481 (Prod. Of Rode Far East)	Polypropylene Glycol	0.05 2.3
	4	Styrene- Crosslinked Isobutylene Based (ITS Polymer Adhesion Grade, Prod. of Kuraray)	30	60	None	Polydimethyl Siloxane	0.07 1.6
	5	Styrene- Crosslinked Isobutylene Based (ITS Polymer Adhesion Grade, Prod. of Kuraray)	30	60	None	Liquid Paraffin	0.2 2.8
	6	Styrene- Isobutylene Based (TS Polymer Adhesion Grade, Prod. of Kuraray)	30	60	None	Polyethylene Glycol	0.5 5.5
	7	Styrenic (Rabalon, Prod. of Mitsubishi Chemical)	400	60	Loaded, 5% Hydroxy- Modified Polyolefin	Ethylen Oxide- Propylene Oxide Copolymer	0.03 4.0
	8	Styrene-Ester Based (Primalloy A, Prod. of Mitsubishi Chemical)	400	60	None	Alcohol Modified Silicone Oil	0.03 4.0

9	Olefin-Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan)	50	60	Applied, Chemlock481 (Prod. Of Rode Far East)	Ethylen Oxide-Propylene Oxide Copolymer	0.03	1.3
10	Styrene-Isobutylene Based (TS Polymer, Prod. of Kuraray)	30	60	Loaded, 5% Ethylene-Vinyl Alcohol Copolymer	Liquid Polybutene	0.63	3.3
11	Styrene-Crosslinked Isobutylene Based (ITS Polymer, Prod. of Kuraray)	30	45	None	2-Ethyl Hexyl Phthalate	0.63	6.9
12	Styrene-Isobutylene Based (TS Polymer Adhesion Grade, Prod. of Kuraray)	30	60	None	Polydimethyl Siloxane	0.14	1.7
13	1) 65% Olefin-Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 30% Styrene-Urethane Based (SU Polymer, Prod. of Kuraray) 3) 5% Styrene-Hydrogenated Isoprene Based (Hybrar, Prod. of Kuraray)	90	50	None	Polydimethyl Siloxane	0.14	5.1

1) * Approximate Oxygen Permeability Coefficient:

Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

2) * Shore Hardness

3) * Value for Relationship(1):

Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

5

Table 3

		Needle Cannula Penetrating Portion/ Fitting Portion			Adhesion Promoter	Applied Lubricant	Sd/ So	3) *
		Material Type (Thermoplastic Elastmer)	1) *	2) *				
Ex.	14	1) 50% Styrene- Isobutylene Based (TS Polymer, Prod. of Kuraray) 2) 50% Styrene- Urethane Based (SU Polymer, Prod. of Kuraray)	90	40	None	Polydimethyl Siloxane	0.08	2.9
	15	1) 50% Olefin- Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 45% Styrene- Urethane Based (SU Polymer, Prod. of Kuraray) 3) 5% Styrene- Hydrogenated Isoprene Based (Hybrar, Prod. of Kuraray)	90	50	None	Polydimethyl Siloxane	0.31	7.0
	16	Styrenic (Rabalon, Prod. of Mitsubishi Chemical)	400	30	Applied, Chemlock481 (Prod. Of Rode Far East)	Polydimethyl Siloxane	0.14	9.4
	17	1) 70% Olefin- Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 30% Styrene- Ester Based (Primalloy A, Prod. of Mitsubishi Chemical)	90	65	None	Polydimethyl Siloxane	0.14	5.1
	18	1) 70% Olefin- Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 30% Styrene- Amide Based (Primalloy E, Prod. of Mitsubishi Chemical)	90	55	None	Polydimethyl Siloxane	0.14	5.1

19	1) 60% Olefin-Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 30% Styrene-Ester Based (Primalloy A, Prod. of Mitsubishi Chemical) 3) 10% Styrene-Urethane Based (SU Polymer, Prod. of Kuraray)	90	60	None	Polydimethyl Siloxane	0.14	5.1
20	Styrenic (Rabalon, Prod. of Mitsubishi Chemical)	400	30	None	Polydimethyl Siloxane	0.03	22.4
21	Styrenic (Rabalon, Prod. of Mitsubishi Chemical)	400	30	None	Polydimethyl Siloxane	0.08	12.6
22	Thermoplastic Silicone (Primer-incorporated, Prod. Of Shinetsu Chemical)	6000	40	None	Polydimethyl Siloxane	0.03	46.0

1) * Approximate Oxygen Permeability Coefficient:
Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

2) * Shore Hardness

5 3) * Value for Relationship(1):
Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

Table 4

	Size										Material Type	1) *	Applied Lubricant
	a	b	c	d	e	f	g	h	i	j			
Comp. Ex.1	10	11	5	4	5	2	13	17	-	-	Crosslinked Butyl Rubber	30	Polydimethyl Siloxane

1) * Approximate Oxygen Permeability Coefficient:

Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

Table 5

		Amount of Absorbed Water (ml)			Needle Cannula Pierceability	Needle Hole Sealability
		Initially	After one Week	Change (%)		
Ex.	1	6.1	5.9	3.3	Satisfactory	Satisfactory
	2	6.1	5.9	3.3	Satisfactory	Satisfactory
	3	6.1	5.8	4.9	Satisfactory	Satisfactory
	4	6.1	5.8	4.9	Satisfactory	Satisfactory
	5	6.0	5.8	3.3	Satisfactory	Satisfactory
	6	6.1	5.8	4.9	Satisfactory	Satisfactory
	7	6.1	5.9	3.3	Satisfactory	Satisfactory
	8	6.0	5.8	3.3	Satisfactory	Satisfactory
	9	6.1	5.8	4.9	Satisfactory	Satisfactory
	10	6.0	5.8	3.3	Satisfactory	Satisfactory
	11	6.1	5.8	4.9	Satisfactory	Satisfactory
	12	6.0	5.8	3.3	Satisfactory	Satisfactory
	13	6.0	5.7	4.9	Satisfactory	Satisfactory
	14	6.0	5.8	3.3	Satisfactory	Satisfactory
	15	6.1	5.8	4.9	Satisfactory	Satisfactory
	16	6.1	5.6	8.0	Satisfactory	Satisfactory
	17	6.0	5.7	4.9	Satisfactory	Satisfactory
	18	6.0	5.8	3.3	Satisfactory	Satisfactory
	19	6.0	5.7	4.9	Satisfactory	Satisfactory
	20	6.0	5.1	15.0	Satisfactory	Satisfactory
	21	6.1	5.4	11.0	Satisfactory	Satisfactory
	22	6.1	4.1	33.0	Satisfactory	Satisfactory
Comp. Ex.1		6.0	5.8	3.3	Satisfactory	Satisfactory

2. EXAMPLES AND COMPARATIVE EXAMPLES CONCERNING THE IMPROVED NEEDLE HOLE SEALABILITY OF THE CLOSURE STRUCTURE

The other embodiments of the present invention will be now described in detail with reference to the following specific examples. The following examples utilize the closure structure embodiment shown in Figure 9. Since the sizes of the closure structure parts, other than the semi-spherical protuberance 8a provided on the needle cannula penetrating portion so as to face toward the blood collection tube, are indicated by the small letters in the same manner as in Figure 12, the explanation thereof is omitted here.

EXAMPLES 23

(Manufacture of Vacuum Blood Collection Tube)

The values for the sizes of closure structure parts as indicated by the small characters shown in Figure 12, their material characteristics and the like are given in Tables 6 and 7. An outer diameter of the semi-spherical protuberance 8a corresponds to the dimension as indicated by the letter a in Figure 12. Twenty vacuum blood collection tubes, each purposed to collect 6 ml blood, were manufactured using the closure structure of this Example in the same manner as in Examples 1 - 19.

(Evaluation)

Each vacuum blood collection tube was caused to suction

collect 30 °C water in the same manner as in Example 1. In order to evaluate its needle hole sealability under severer conditions than in Examples 1 - 19, the vacuum blood collection tube was then completely immersed in a constant temperature water vessel maintained at 40 °C so as to reside in an upright position for 20 seconds, during which time the possible leakage of air bubbles through the needle hole was visually observed.

COMPARATIVE EXAMPLE 2

10 (Manufacture of Vacuum Blood Collection Tube)

Twenty vacuum blood collection tubes, each identical in construction to that of Comparative Example 1 and purposed to collect 6 ml blood, were manufactured.

(Evaluation)

15 The possible leakage of air bubbles through the needle hole was visually observed in the same manner as in Example 23.

COMPARATIVE EXAMPLE 3

(Manufacture of Vacuum Blood Collection Tube)

20 The product specification of Example 23 was followed, except that the semi-spherical protuberance 8a was excluded, to manufacture twenty vacuum blood collection tubes, each purposed to collect 6 ml blood.

(Evaluation)

25 The possible leakage of air bubbles through the needle

hole was visually observed in the same manner as in Example 23.

(Results of Example 23 and Comparative Examples 2, 3)

The results are shown in Tables 6 and 7. In Example 23, the proportion of vacuum blood collection tubes that showed air bubble leakage was determined as being 1/20, as comparable to that determined for Comparative Example 2. In contrast, the proportion of vacuum blood collection tubes in Comparative Example 3 that showed air bubble leakage was determined as being 12/20, although observed under severe conditions. This demonstrate their insufficient needle hole sealability.

Table 6

		Size									Grip Section		
		a	b	c	d	e	f	g	h	i	j	Material Type (Thermoplastic Resin)	1)*
Ex.23		7.6	11	3	1	4	4	5	2	13	17	Polyethylene Terephthalate	1
Comp. EX.	2	Identical to Those of Comp. Ex.1											
	3	7.6	11	3	1	4	4	5	2	13	17	Polyethylene Terephthalate	1

1)* Approximate Oxygen Permeability Coefficient:
Unit in $\times 10^{-10}$ ml/cm²·mm⁻¹·sec·cmHg

Table 7

		Needle Cannula Penetrating Portion/ Fitting Portion		Adhesion Promoter	Applied Lubricant	3) *	4) *
		Material Type (Thermoplastic Elastmer)	1) * 2) *				
Ex.	23	Styrene- Isobutylene Based (TS Polymer Adhesion Grade, Prod. of Kuraray)	30 60	None	Polyethylene Glycol	Present	1/20
5	2	Identical to Those of Comp. Ex. 1					0/20
	3	Styrene- Isobutylene Based (TS Polymer Adhesion Grade, Prod. of Kuraray)	30 60	None	Polyethylene Glycol	Absent	12/20

1) * Approximate Oxygen Permeability Coefficient:
Unit in $\times 10^{-10} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$

2) * Shore Hardness

3) * Semi-Spherical Protuberance

4) * Frequency of Air Bubble Leakage

3. EXAMPLES/COMPARATIVE EXAMPLES CONCERNING THE VACUUM BLOOD COLLECTION DEVICE HOLDER

EXAMPLE 24

(Manufacture of a Vacuum Blood Collection Device
Holder)

Polyoxymethylene was injection molded to form a spring-
like elastic member 64, such as shown in Figure 13(a), as a
separate member which can be built in a main body of the
holder for vacuum blood collection devices, as illustrated
in Figure 16(b). This elastic member was fittingly placed

in a position deep inside a generally marketed polypropylene vacuum blood collection device holder as illustrated in Figure 18(b). Figure 16(a) is a partially cut-away sectional view of the resulting vacuum blood collection device holder.

(Evaluation)

A vacuum blood collection tube similar in construction to that of Example 1 and a 21G multiple blood collection needle were fittingly coupled to the holder of this Example. Then, suction was applied to collect 30 °C water in the tube, as similar to Examples 1 - 19, to visually observe the kickback preventive performance during the suction.

(Results)

The insertion of the vacuum blood collection tube deep inside the holder resulted in the elastic engagement of the kickback preventive annular rib disposed in the grip section of the closure structure with the groove on the kickback preventive elastic member disposed deep inside the holder. This engagement was sufficient to withstand a counterforce accompanying compression of the elastic sheath of the multiple blood collection needle, so that the vacuum blood collection tube was allowed to be kept retained within the holder 60 in a satisfactory fashion. After the suction was terminated, a sufficient pulling force was applied to the blood collection tube. Then, the annular rib failed to

resist the force to disengage from the groove 64a, resulting in the successful separation of the blood collection tube from the holder.

COMPARATIVE EXAMPLE 4

5 (Manufacture of a Vacuum Blood Collection Device Holder)

A generally marketed polypropylene, vacuum blood collection device holder that excluded a kickback preventive member, as shown in Figure 18(b), was used without any
10 modification.

(Evaluation)

Evaluation was performed in the same manner as in Example 24.

(Results)

15 As the vacuum blood collection tube of the present invention was brought deeper inside the holder, the counterforce of the rubber sheath of the multiple blood collection needle increased. The associated increase of the kickback force made it difficult to continue collecting
20 water by suction without the assistance of a finger tip to apply a force toward a bottom of the blood collection tube.

4. EXAMPLES/COMPARATIVE EXAMPLES RELATING TO THE COMPOUNDING MATERIAL WHICH SUPPRESS THE ELUTION OF METAL IONS FROM THERMOPLASTIC ELASTOMER CONTAINING TRANSITION METAL OXIDE AS
25 A CATALYST FOR DYNAMIC CROSSLINKING

EXAMPLES 25 AND 26

(Preparation of Pellet-Form Compounding Material)

The compounding additives used are specified in Table 8. In Example 25, ethylene-methacrylate copolymer (NUCREL, manufactured by Mitsui-Du Pont Polychemical Co., Ltd.) was used as an additive for formation of insoluble metal salts. In Example 26, styrene/amide thermoplastic elastomer (PRIMALLOY E, manufactured by Mitsubishi Chemical Co., Ltd.) was used as an additive for formation of insoluble metal chelates. The dynamic crosslinking catalyst used for olefin/crosslinked isobutylene thermoplastic elastomer (TREFSIN, manufactured by AES Japan Ltd.) was zinc oxide. The compounding additives were roughly mixed by stirring and then melt kneaded by using an extruder. The extruded strands were subsequently cooled in water. Finally, a compounding material was obtained in the pellet form.

(Evaluation)

The pellet-form compounding material was immersed in ten-fold weight of ion-exchanged water and maintained at 40 °C for 24 hours. Thereafter, a concentration of zinc in the ion-exchanged water was determined by atomic absorption spectroscopy.

COMPARATIVE EXAMPLE 5

(Preparation of Pellet-Form Compounding Material)

The pellet-form olefin/crosslinked isobutylene

thermoplastic elastomer (TREFSIN, manufactured by AES Japan Ltd.) was used.

(Evaluation)

Evaluation was performed in the same manner as in
5 Examples 25 and 26.

(Results of Examples 25, 26 and Comparative Example 5)

The zinc concentration determined for each Example was divided by the loading proportion of the olefin/crosslinked isobutylene thermoplastic elastomer (TREFSIN, manufactured
10 by AES Japan Ltd.) and further divided by the concentration of zinc determined for Comparative Example 5 to give a relative value when the concentration of eluted zinc in Comparative Example 5 was taken as 1.0. The results are given in Table 9. The concentration of eluted zinc
15 determined for each Example was reduced to about a quarter of that for Comparative Example 5, demonstrating the improved effect.

Table 8

	Formulation Ingredients
Ex.25	1) 57% Olefine-Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 35% Styrene-Ester Based (Primalloy A, Prod. of Mutsubishi Chemical) 3) 5% Styrene-Urethane Based (SU Polymer, Prod. of Kuraray) 4) 3% Ethylene-Methacrylic Acid Copolymer (Nucrel, Prod. of Mitsui-Dupont Polychemical)
Ex.26	1) 70% Olefine-Crosslinked Isobutylene Based (Trefsin, Prod. of AES Japan) 2) 30% Styrene-Amide Based (Primalloy E, Prod. of Mitsubishi Chemical)

Table 9

	Conc. of Eluted Zinc
Ex.25	0.22
Ex.26	0.25
Comp.Ex.5	1.00

UTILITY IN INDUSTRY

The closure structure for a vacuum specimen collection container according to the first invention is constructed to include the grip section, the rubber elastic needle cannula penetrating portion and the rubber-like elastic fitting portion, and the reduction in structural complexity leads to its high productivity. Also, at least one recessed or raised portion for a kickback preventive purpose is provided

on an inner side of the tubular side wall portion in the grip section. If a raised or recessed portion engageable with the aforementioned recessed or raised portion is provided deep inside a needle cannula retaining portion of the vacuum specimen collection device holder, the occurrence of a kickback phenomenon which may be caused, for example, by an elastic sheath of a multiple blood collection needle, is prevented effectively.

Also, the rubber-like elastic fitting portion is configured to be fittingly received in an airtight fashion by an inner surface of an open end of a specimen collection tube, thereby assuring the effective maintenance of a vacuum condition within the vacuum specimen collection container.

The ability of the needle cannula penetrating portion to permit easy penetration of a needle cannula and reseal a needle hole left after it is retracted is also contributive to maintaining a sealed condition of the vacuum specimen collection container.

In the embodiment where the closure structure for a vacuum specimen collection container according to the first invention further includes a fitting portion supporting member embedded in the fitting portion, the integrity of the fitting portion within the closure structure is increased to thereby prevent excessive deformation of the elastic fitting portion that may be caused when the closure structure is

attached or detached.

In addition, the reduction in needle hole sealability as a result of the provision of the fitting portion supporting member can be suppressed by the provision of the protuberance on a bottom surface of the needle cannula penetrating portion. That is, the provision of protuberance on the bottom surface of the needle cannula penetrating portion enhances the needle hole sealability in the manner as described earlier.

The closure structure for a vacuum specimen collection container according to the second invention is constructed to include the grip section, the rubber elastic needle cannula penetrating portion and the rubber-like elastic fitting portion, as similar to the first invention, and the reduction in structural complexity leads to its high productivity. Also, the provision of the protuberance on the bottom surface of the needle cannula penetrating portion increases the needle hole sealability to thereby effectively maintain a sealed condition of the vacuum specimen collection container.

In the vacuum specimen collection container closure structure according to the present invention, if the through-hole is configured to increase its diameter in an upward direction from the needle cannula penetrating portion, the introduction such as of a vacuum blood

collection needle or a sampling nozzle for specimen extraction into the through-hole can be facilitated. This accordingly leads to the easy introduction of their tips into the vacuum specimen collection container.

5 If a wall thickness $T1$ (mm) of the partition portion of the grip section, an oxygen permeability coefficient $P1$ ($\text{ml}/\text{cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$) of the partition portion at $25\text{ }^\circ\text{C}$, a wall thickness $T2$ (mm) of the needle cannula penetrating portion in a needle penetrating direction, an oxygen
10 permeability coefficient $P2$ ($\text{ml}/\text{cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$) of the needle cannula penetrating portion at $25\text{ }^\circ\text{C}$, a minimum cross-sectional area Sd (cm^2) of the through-hole in the grip section and an open area So (cm^2) at the open end of the specimen collection tube are selected to satisfy the
15 relationship (1), the gas barrier property of the closure structure is enhanced to a sufficient level to effectively maintain a vacuum condition within the vacuum specimen collection container.

 The vacuum specimen collection container closure
20 structure according to the present invention, if its grip section is formed from the above-specified thermoplastic resin composition and its needle cannula penetrating portion and fitting portion are formed from the above-specified respective thermoplastic elastomer compositions and Sd/So
25 does not exceed 0.7, can effectively maintain a vacuum

condition within the vacuum specimen collection container because of its excellent gas barrier property. Also, the use of the thermoplastic resin and elastomer compositions allows easy manufacture of the closure structure such as by
5 injection molding, thereby increasing productivity of the closure structure for a vacuum specimen collection container.

If the grip section is comprised principally of at least one selected from the group consisting of polyester,
10 polyamide, polyallylate, polyacetal and ethylene-vinyl alcohol copolymer, and the needle penetrating portion and the fitting portion are comprised of thermoplastic elastomer that can be chemically or thermally adhered to the grip section, the closure structure can effectively maintain a
15 vacuum condition within the vacuum specimen collection container as a result of its excellent gas barrier property. In addition, the easy connection of the needle cannula penetrating portion and fitting portion to the grip section by chemical or thermal adhesion increases productivity of
20 the closure structure for a vacuum specimen collection container.

A vacuum specimen collection container according to the present invention includes the closure structure of the present invention and a vacuum specimen collection tube.
25 Due to the incorporation of the closure structure excellent

in productivity and gas barrier property, the vacuum specimen collection container has the capability to surely maintain its interior pressure if reduced to vacuum.

In the case where a vacuum specimen collection
5 container according to the present invention includes a closure structure according to the second invention and a vacuum specimen collection tube having a rubber-like elastic, closure structure receiving portion at an inner
10 face of its opening, the provision of the rubber-like elastic, closure structure receiving portion in the vacuum specimen collection tube facilitates insertion of the closure structure into the vacuum specimen collection tube and permits the closure structure fitting portion to come into close contact with the inner face at the opening of the
15 vacuum specimen collection tube.

A vacuum specimen collection system according to the present invention includes a closure structure for a vacuum specimen collection container according to the present invention, a vacuum specimen collection tube, a vacuum
20 specimen collection device holder and a vacuum specimen collection needle. Also, an elastic member having a raised or recessed portion engageable with the recessed or raised portion on an inner side of the tubular side wall portion in the grip section of the closure structure is provided deep
25 inside a needle cannula retaining portion of the vacuum

specimen collection device holder. This effectively prevents the occurrence of the above-described kickback phenomenon which may be caused when a multiple vacuum specimen collection needle is used, as well as leading to the construction of the vacuum specimen collection system excellent in productivity and gas barrier property.

A vacuum specimen collection device holder according to the present invention is the holder for use in combination with a closure structure according to the present invention. Since it incorporates an elastic member having a raised or recessed portion engageable with the recessed or raised portion on an inner side of the tubular side wall portion in the grip section of the closure structure, the occurrence of the above-described kickback phenomenon that may be caused when used in combination with a multiple vacuum specimen collection needle can be effectively prevented.

A thermoplastic elastomer composition according to the present invention is utilized to form at least a needle cannula penetrating portion and a rubber-like elastic fitting portion of a closure structure for a vacuum blood collection container according to the present invention. In such a case, a transition metal is caused to form a water-insoluble salt or chelate so that its ionic form dissolution into the specimen is effectively prevented.

C L A I M S

1. A closure structure for a vacuum specimen collection container which can be detachably fitted in an open end of a specimen collection tube in an airtight manner to maintain a vacuum condition inside the specimen collection tube, the closure structure being characterized as comprising:

a grip section including a tubular side wall portion for providing a finger grip, a partition portion extending inward from the side wall portion and having a through-hole through which a specimen collection needle cannula can be passed into the specimen collection tube;

a rubber elastic, needle cannula penetrating portion provided to fill up the through-hole in the grip section and having the capability to reseal a hole if left after the needle cannula is retracted;

a rubber-like elastic fitting portion depending from the needle cannula penetrating portion or the grip section and configured to follow an inner surface profile at the open end of the specimen collection tube to thereby contact fit therein in an airtight manner;

said grip section having a higher rigidity relative to the needle cannula penetrating portion and the fitting portion; and

said tubular side wall of the grip section being

provided on its inner side with at least one raised or recessed portion for kickback preventive purpose.

2. The closure structure for a vacuum specimen collection container as recited in claim 1, characterized as
5 further comprising a fitting portion supporting member extending from the partition portion toward the fitting portion and embedded in the fitting portion, and a protuberance provided on a bottom surface of the needle cannula penetrating portion that is located above a lower
10 end of the fitting portion supporting member.

3. A closure structure for a vacuum specimen collection container which can be detachably fitted in an open end of a specimen collection tube in an airtight manner to maintain a vacuum condition inside the specimen collection tube, the
15 closure structure being characterized as comprising:

a grip section including a tubular side wall portion for providing a finger grip, a partition portion extending inward from the side wall portion and having a through-hole through which a specimen collection needle cannula can be
20 passed into the specimen collection tube;

a rubber elastic, needle cannula penetrating portion provided to fill up the through-hole in the grip section and having the capability to reseal a hole if left after the needle cannula is retracted;

25 a rubber-like elastic fitting portion depending from

the needle cannula penetrating portion or the grip section and configured to follow an inner surface profile at the open end of the specimen collection tube to thereby contact fit therein in an airtight manner; and

5 said needle cannula penetrating portion being provided on its bottom surface with a protuberance.

4. The closure structure for a vacuum specimen collection container as recited in any one of claims 1 - 3, wherein said through-hole is configured to increase its diameter in an upward direction from the needle cannula penetrating portion.

5. The closure structure for a vacuum specimen collection container as recited in any one of claims 1 - 4, wherein below-specified parameters satisfy the following relationship (1):

$$\frac{(S_o - S_d) \times P_1}{T_1} + \frac{S_d \times P_2}{T_2} \leq 1.0 \times 10^{-10} \quad \dots (1)$$

where T1 (mm) is a wall thickness of the partition portion of the grip section, P1 (ml/cm²·mm⁻¹·sec·cmHg) is an oxygen permeability coefficient of the partition at 25 °C, T2 (mm) is a wall thickness of the needle cannula penetrating portion in a needle penetrating direction, P2 (ml/cm²·mm⁻¹·sec·cmHg) is an oxygen permeability coefficient of the needle cannula penetrating portion at 25 °C, Sd (cm²) is a

minimum cross-sectional area of the through-hole in the grip section and S_o (cm^2) is an open area at the open end of the specimen collection tube.

5 6. The closure structure for a vacuum specimen collection container as recited in claim 5, wherein the grip section comprises a thermoplastic resin composition having an oxygen permeability coefficient at 25 °C, P_1 , of not exceeding $30 \times 10^{-1} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$, the needle cannula penetrating portion comprises a thermoplastic elastomer
10 composition having an oxygen permeability coefficient at 25 °C, P_2 , of not exceeding $700 \times 10^{-1} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$, and the fitting portion comprises a thermoplastic elastomer composition having an oxygen permeability coefficient at 25 °C of not exceeding $10,000 \times 10^{-1} \text{ ml/cm}^2 \cdot \text{mm}^{-1} \cdot \text{sec} \cdot \text{cmHg}$; and
15 wherein a ratio of a minimum cross-sectional area S_d of the through-hole in the grip section to an open area S_o at the open end of the specimen collection tube, S_d/S_o , does not exceed 0.7.

20 7. The closure structure for a vacuum specimen collection container as recited in any one of claims 1 - 6, wherein the grip section is comprised principally of at least one selected from the group consisting of polyester, polyamide, polyallylate, polyacetal and ethylene-vinyl alcohol copolymer, and wherein the needle penetrating
25 portion and the fitting portion are comprised of

thermoplastic elastomer that can be chemically or thermally adhered to the grip section.

8. A vacuum specimen collection container including the closure structure as recited in any one of claims 1 - 7, and
5 a vacuum specimen collection tube.

9. A vacuum specimen collection container including the closure structure as recited in claim 3, and a vacuum specimen collection tube having a rubber-like elastic, closure structure receiving portion at an inner face of its
10 open end.

10. A vacuum specimen collection system characterized as including:

the closure structure for a vacuum specimen collection container as recited in any one of claims 1 - 7;

15 a vacuum specimen collection tube;

a tubular holder having an opening at its one end for receiving the vacuum specimen collection tube and a means at its another end for retaining a specimen collection needle cannula;

20 a vacuum specimen collection needle; and

an elastic member provided deep inside the holder on the needle cannula retaining side and having a recessed or raised portion which is engageable with the raised or recessed portion provided on the inner side of the tubular
25 side wall in the grip section of the closure structure.

11. A holder for use in combination with the closure structure for a vacuum specimen collection container as recited in any one of claims 1 - 7, characterized in that said holder is tubularly configured to have an opening at
5 its one end for receiving a vacuum specimen collection tube and a means at its another end for retaining a specimen collection needle cannular, and that said holder is provided deep inside thereof on the needle cannula retaining side with a recessed or raised portion engageable with the raised
10 or recessed portion on the inner side of the tubular side wall in the grip section of the closure structure.

12. A thermoplastic elastomer composition for use in the formation of at least the needle cannula penetrating portion and/or the rubber-like elastic fitting portion of
15 the closure structure as recited in any one of claims 1 - 7, said composition containing thermoplastic elastomer having rubber elastic domains produced via dynamic crosslinking under a catalyzing action of transition metal oxide, and a compound capable of forming a water-insoluble salt or
20 chelate with said transition metal.

FIG. 1

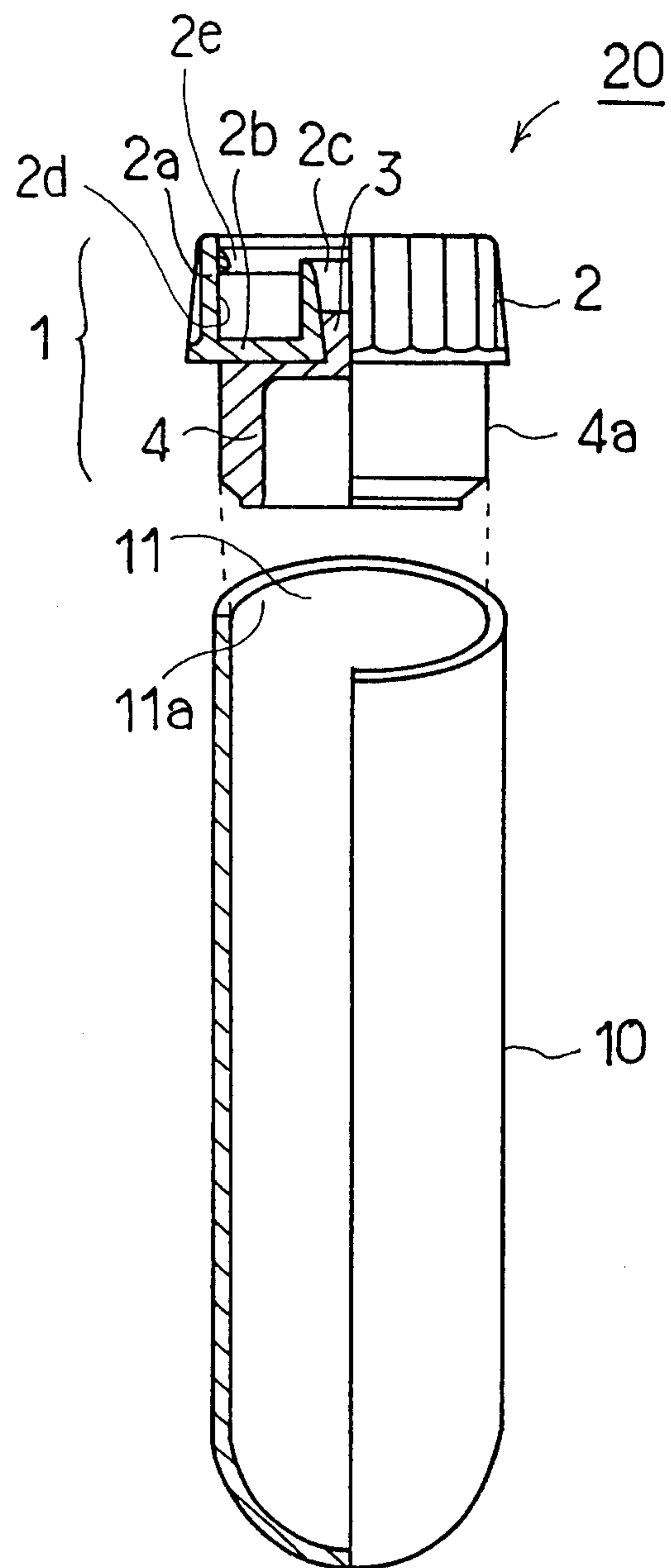


FIG. 2

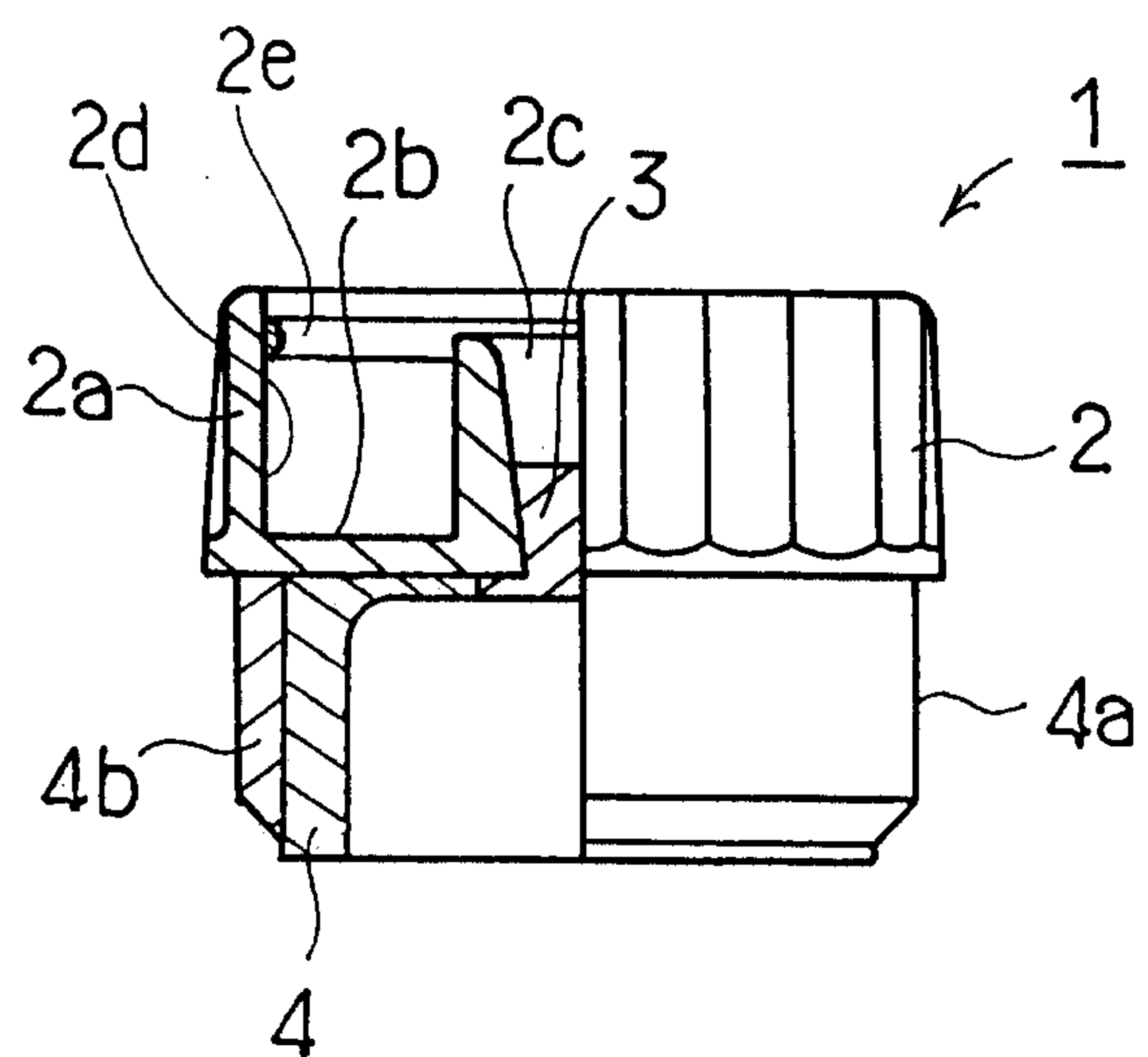


FIG. 3

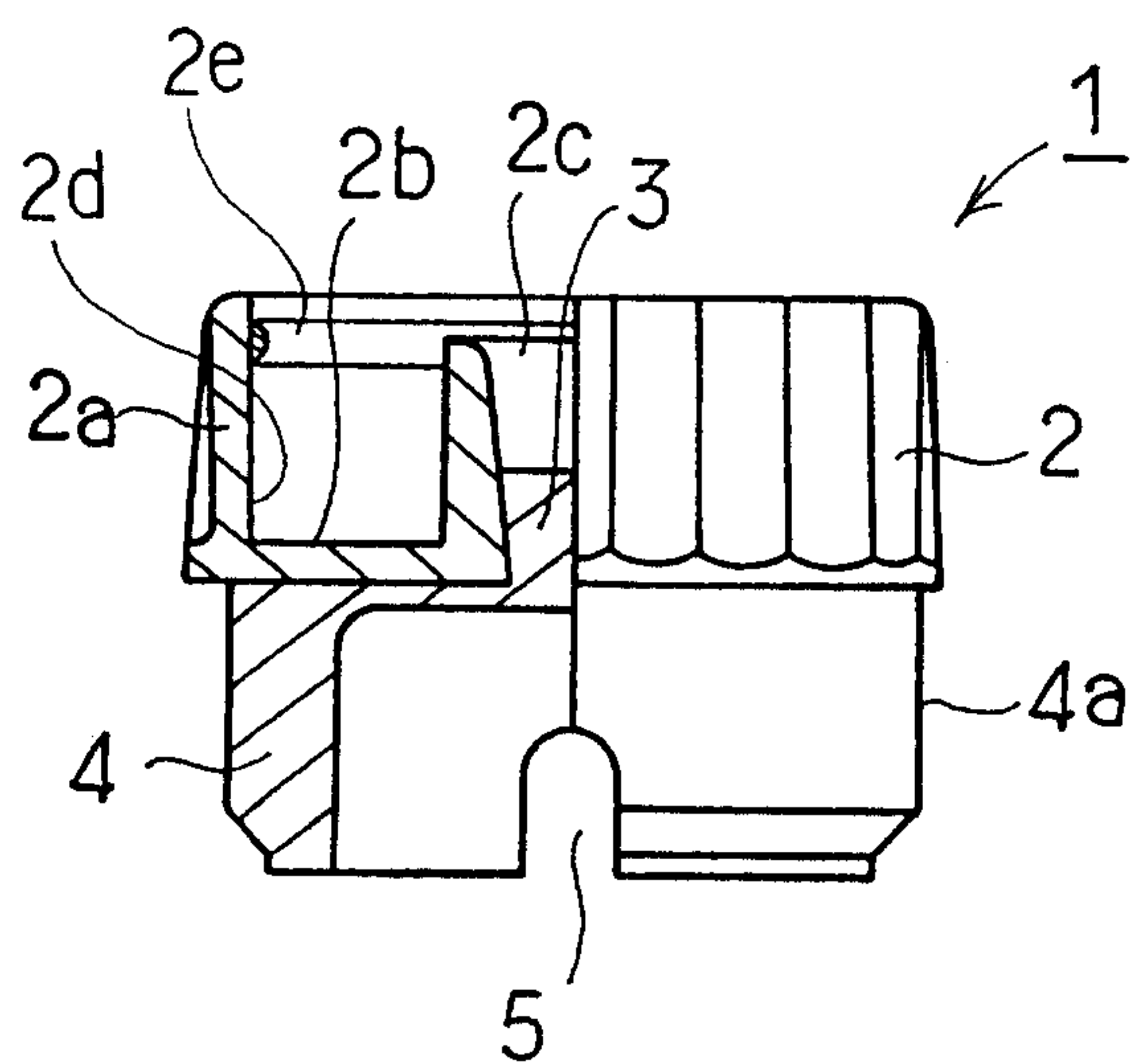


FIG. 4

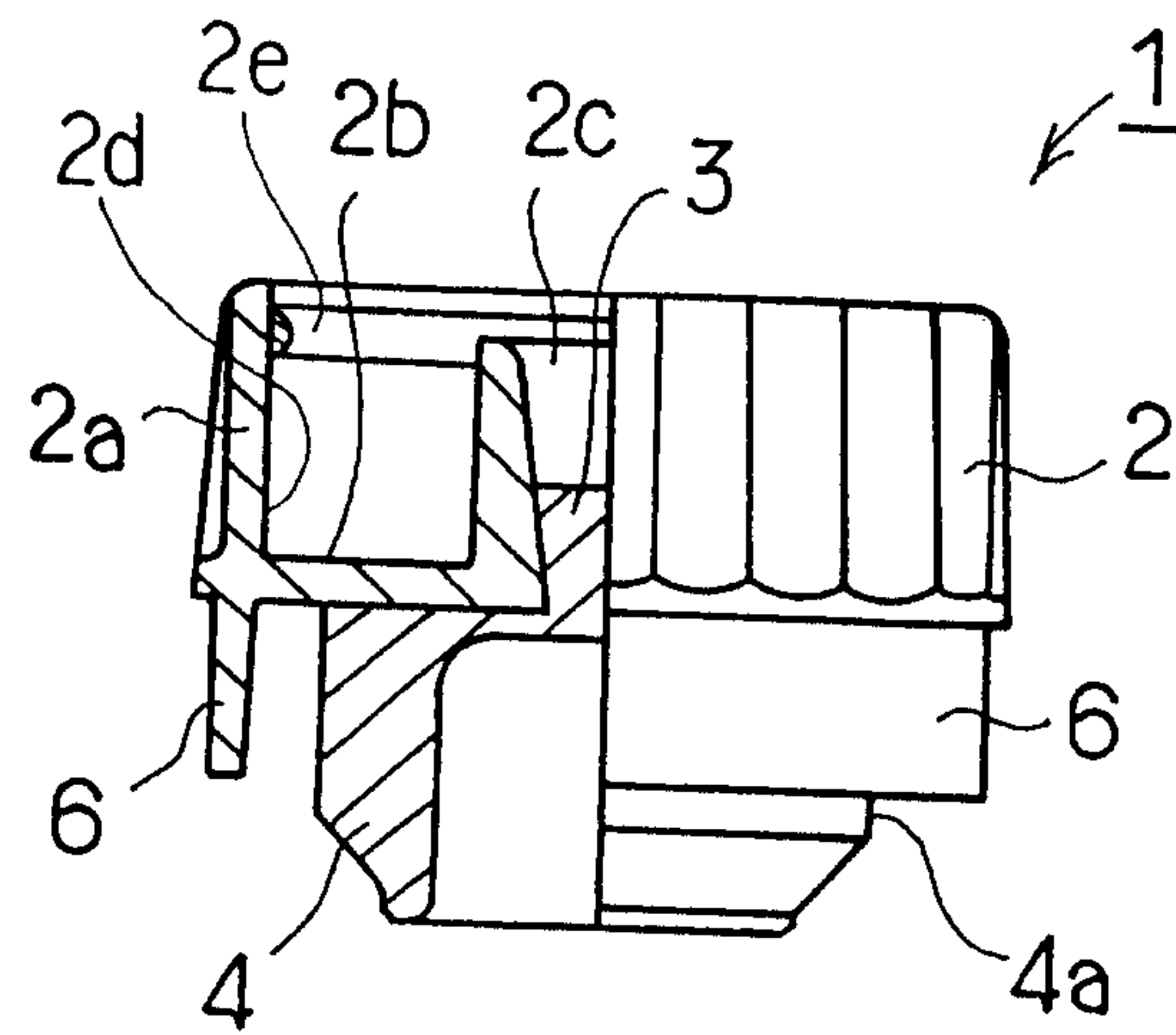


FIG. 5

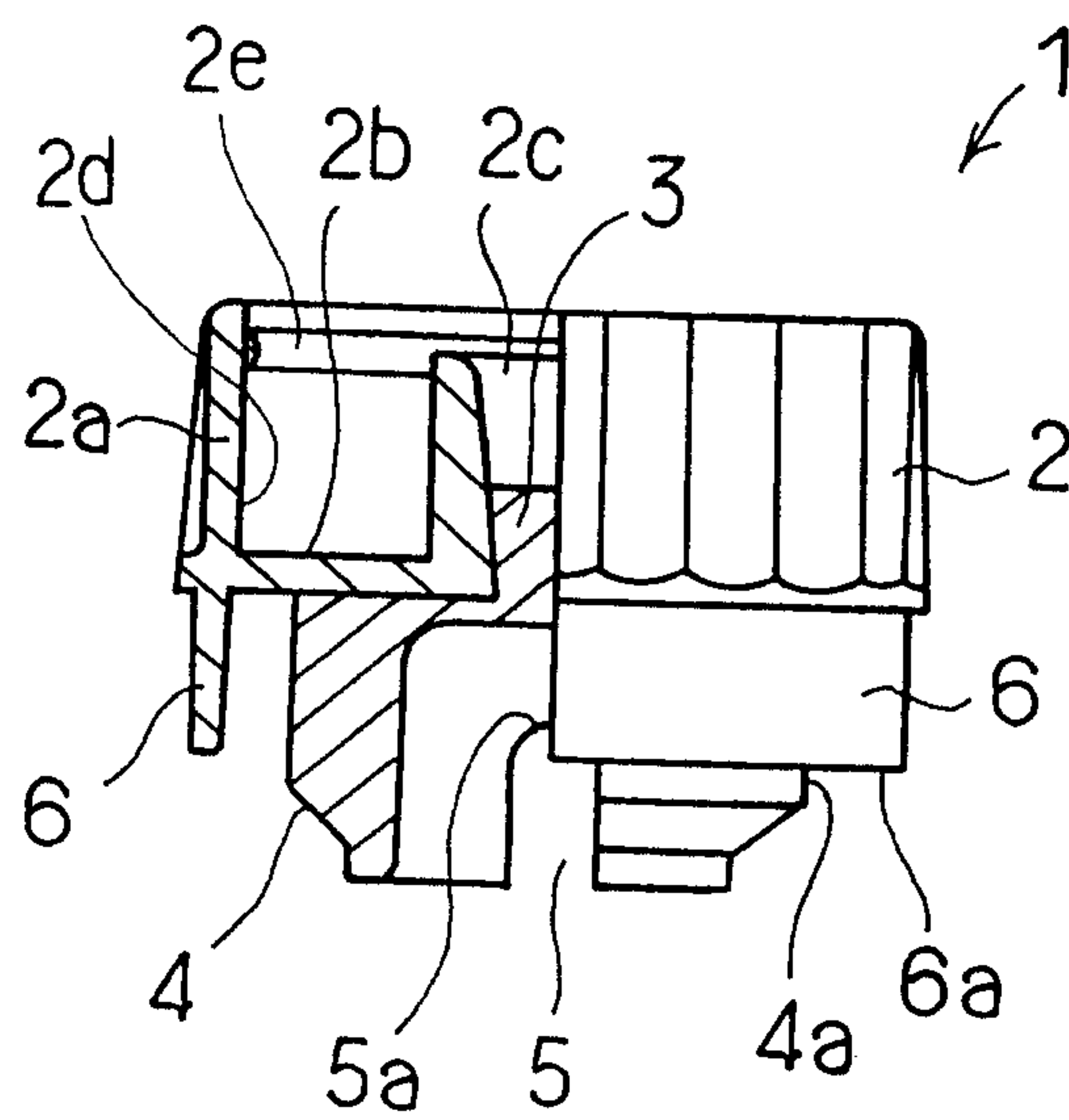


FIG. 6

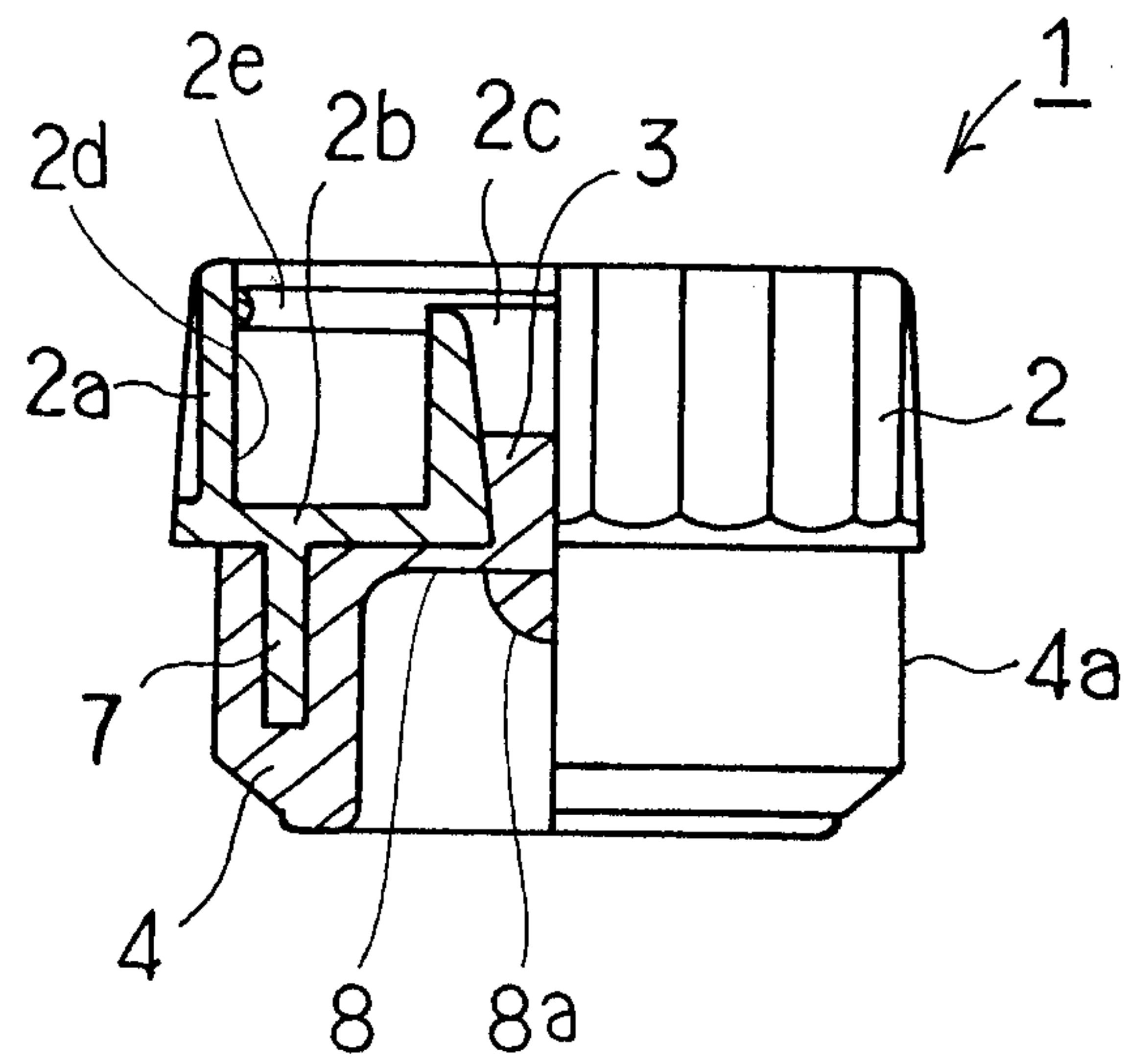


FIG. 7

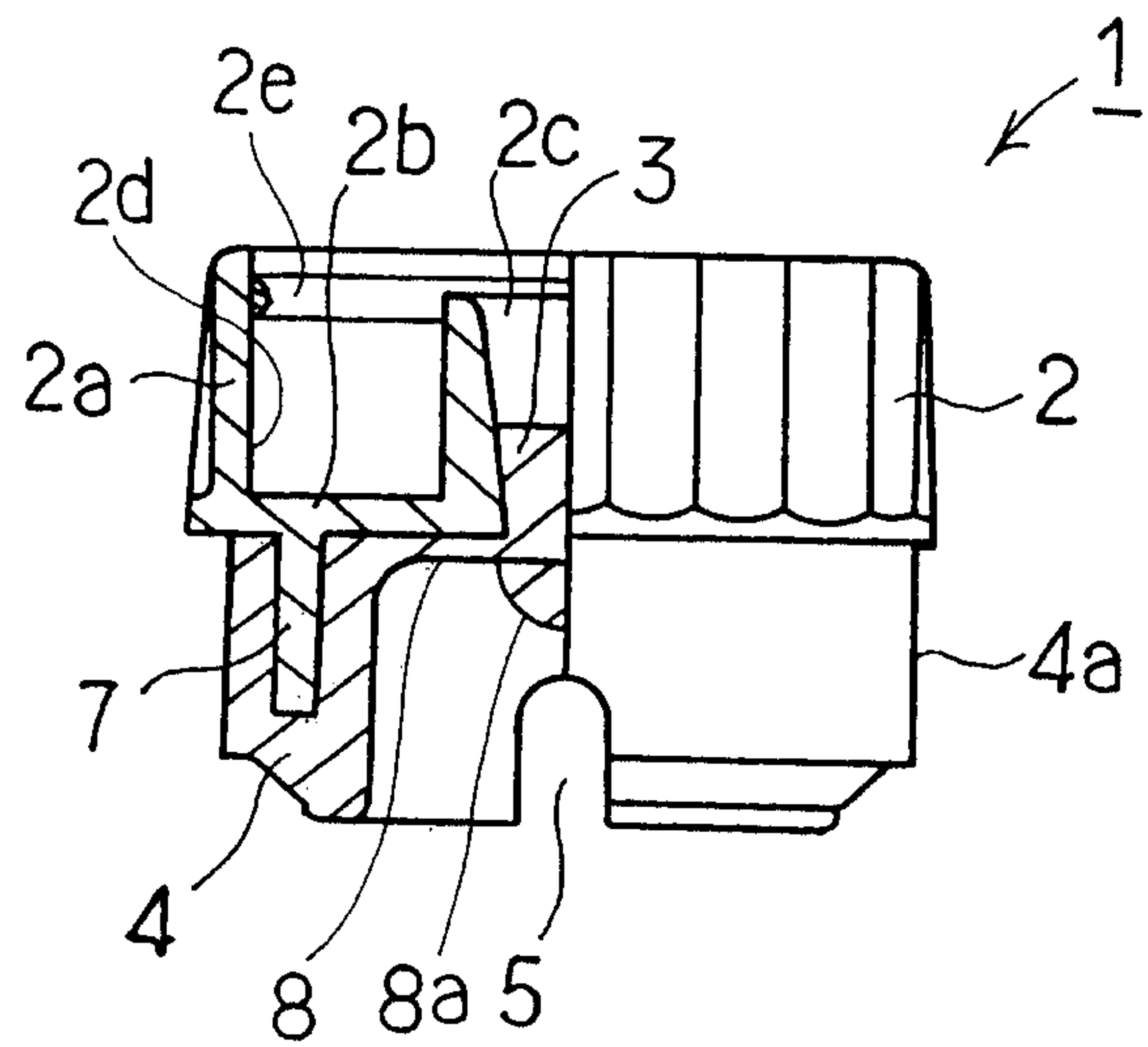


FIG. 8

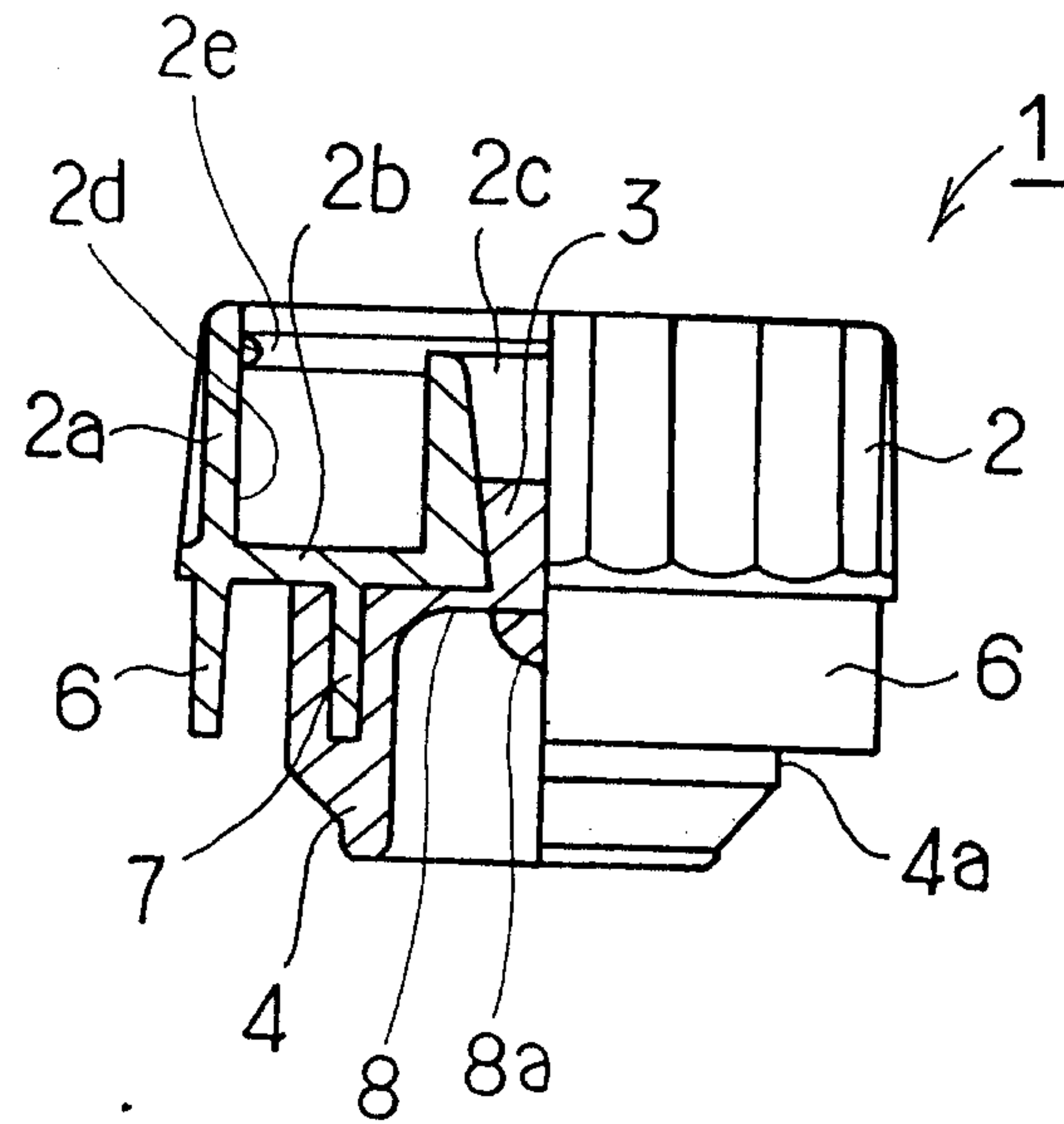


FIG. 9

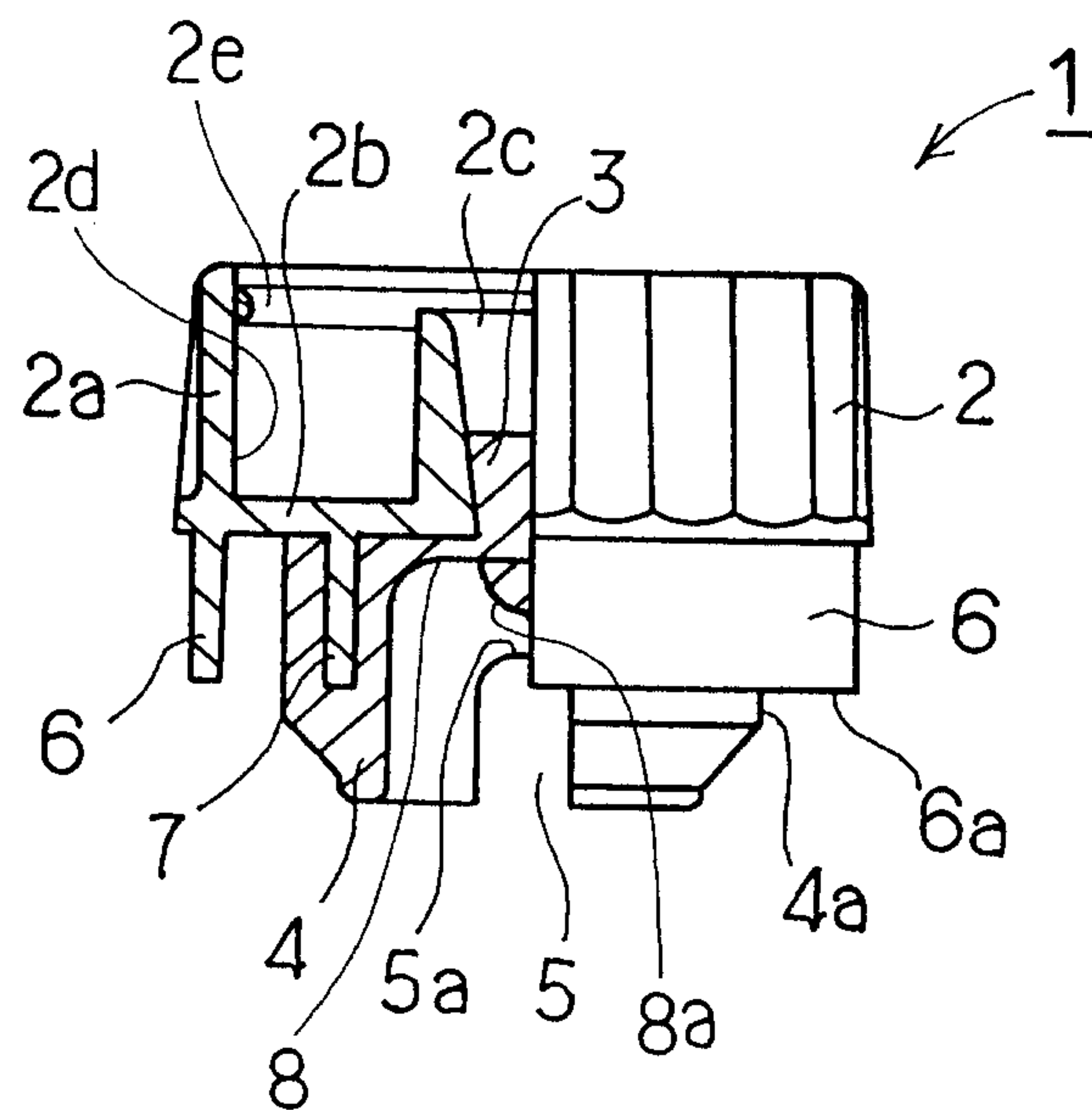


FIG. 10

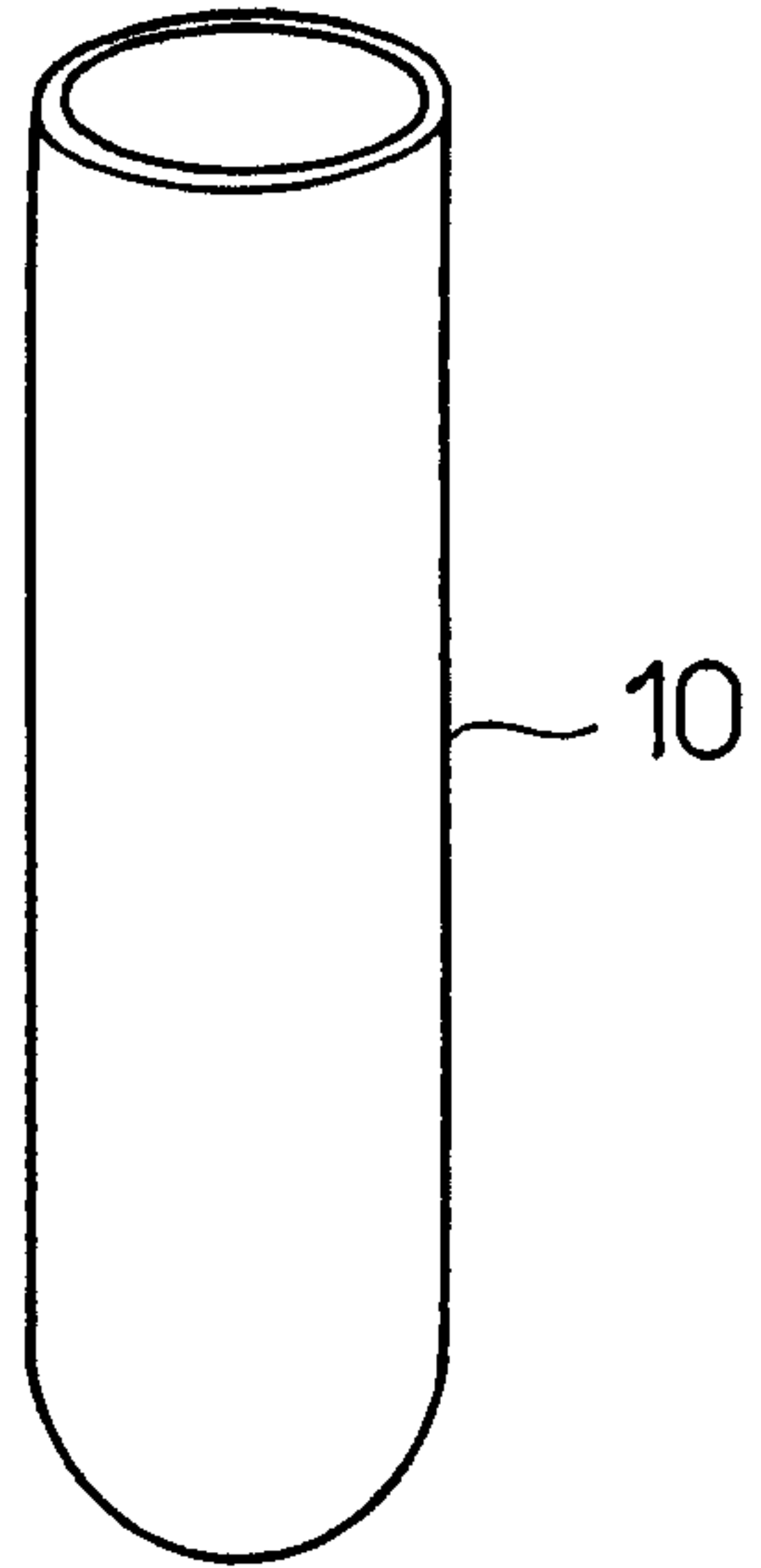


FIG. 11

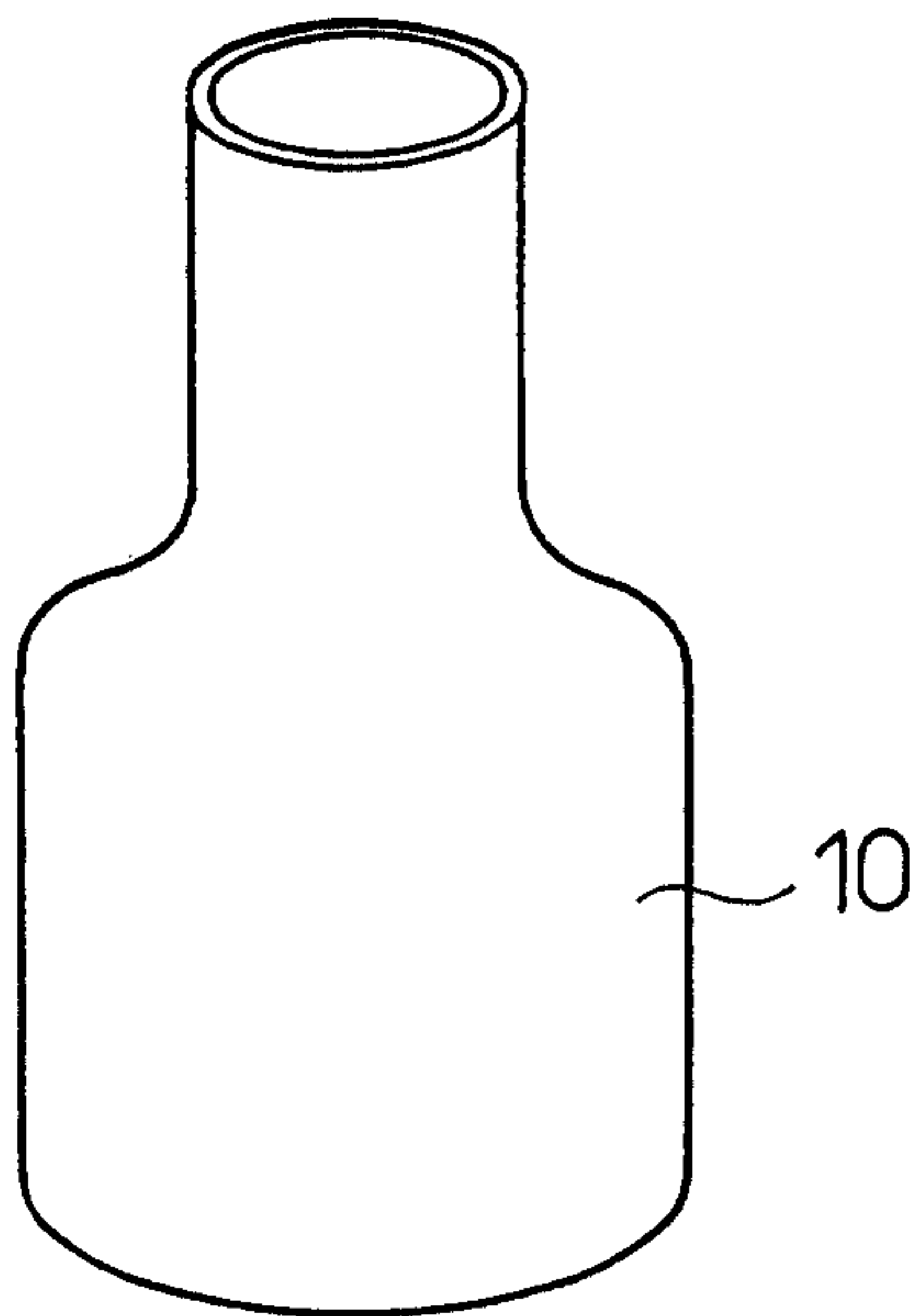


FIG. 12

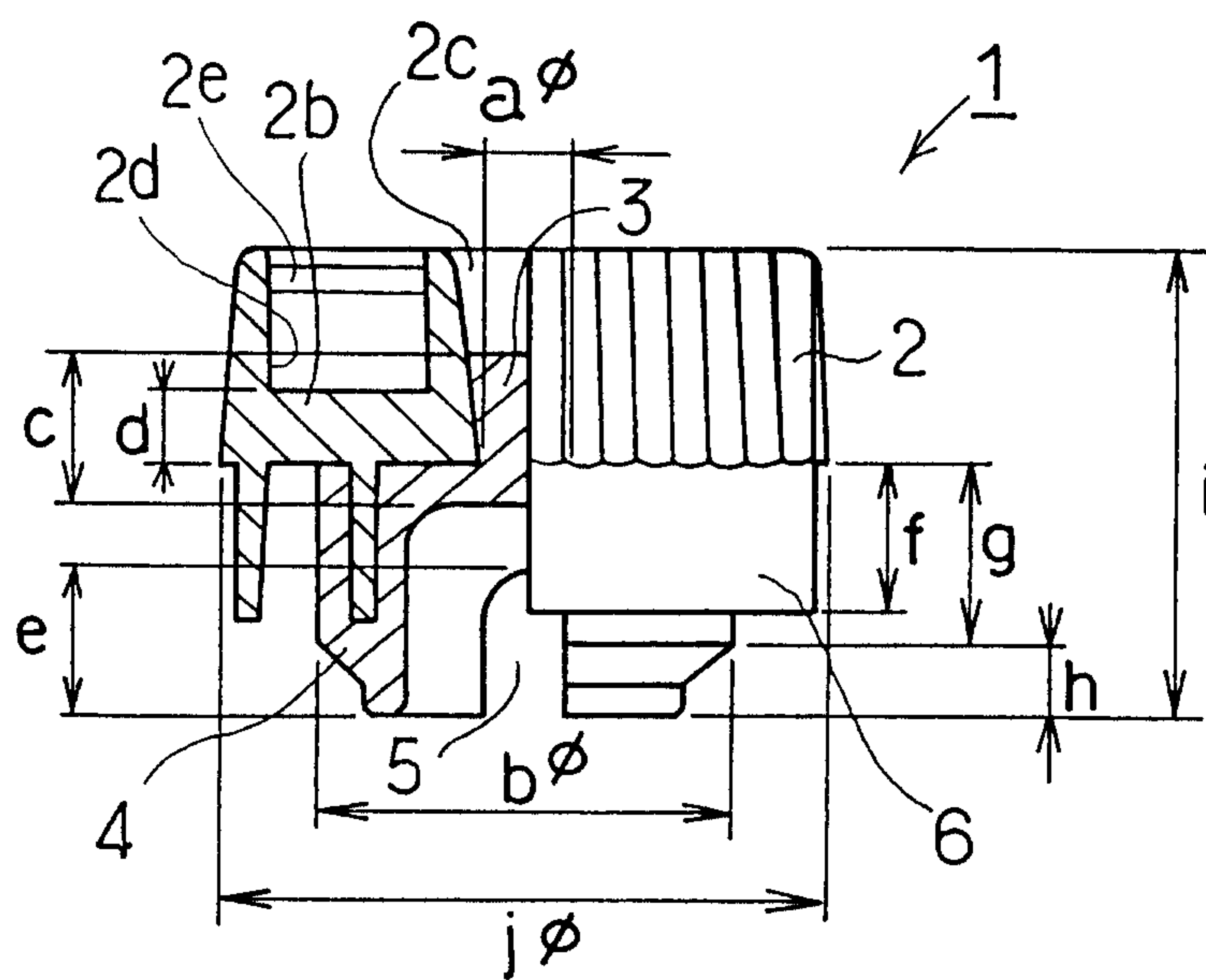


FIG. 13

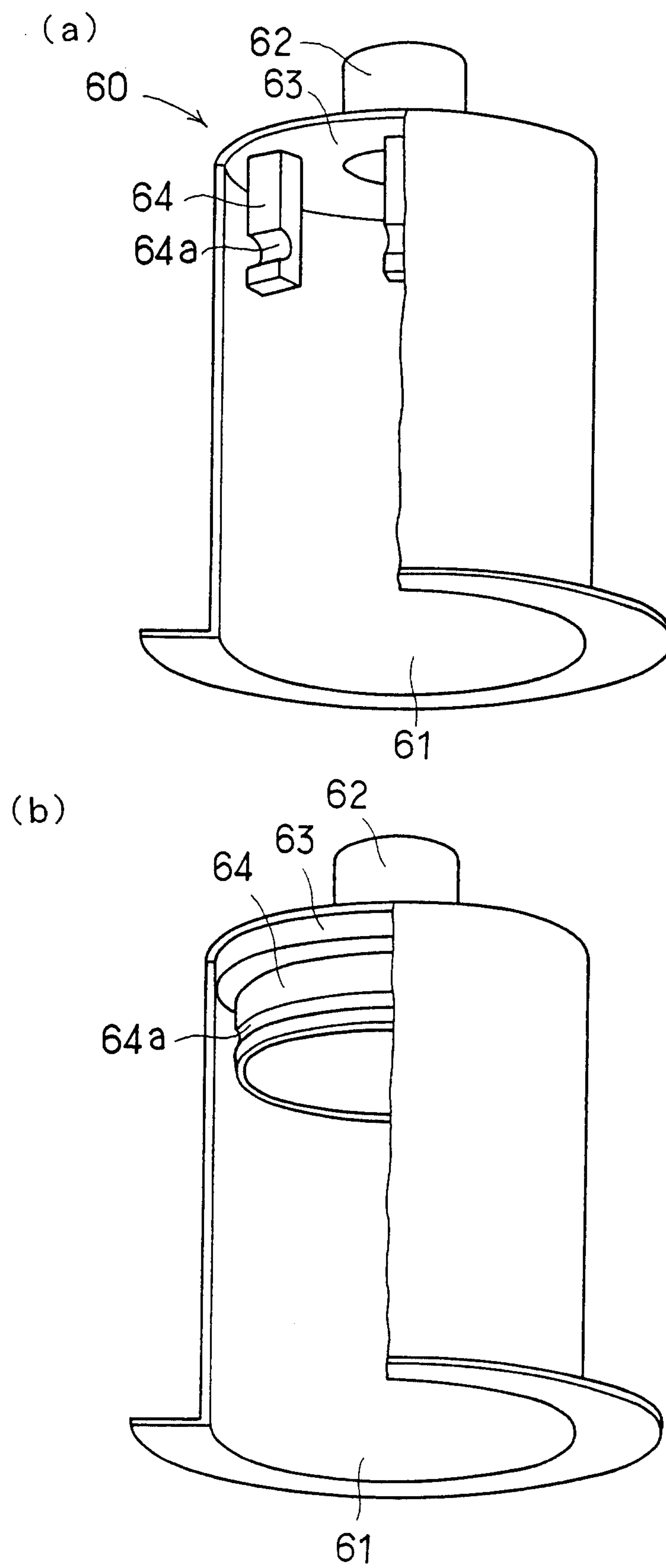


FIG. 14

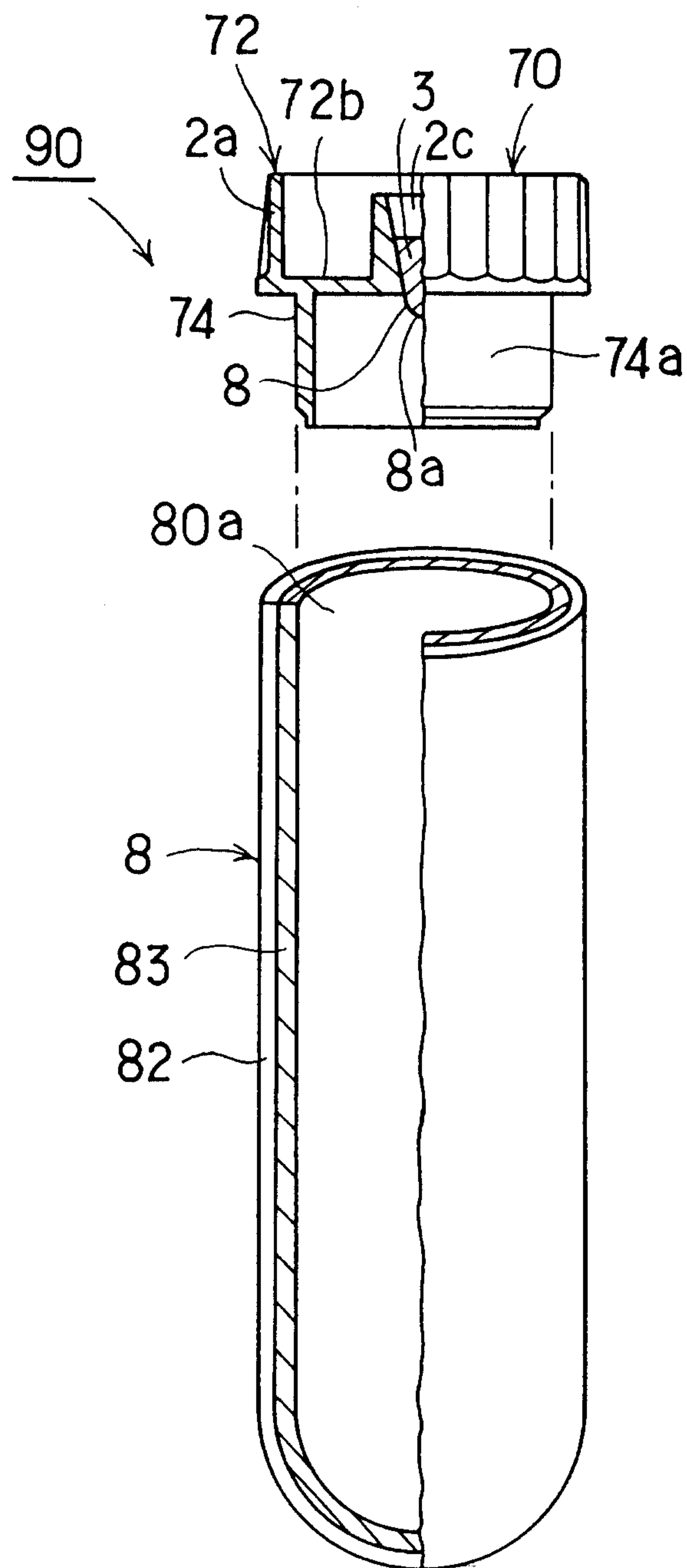


FIG. 15

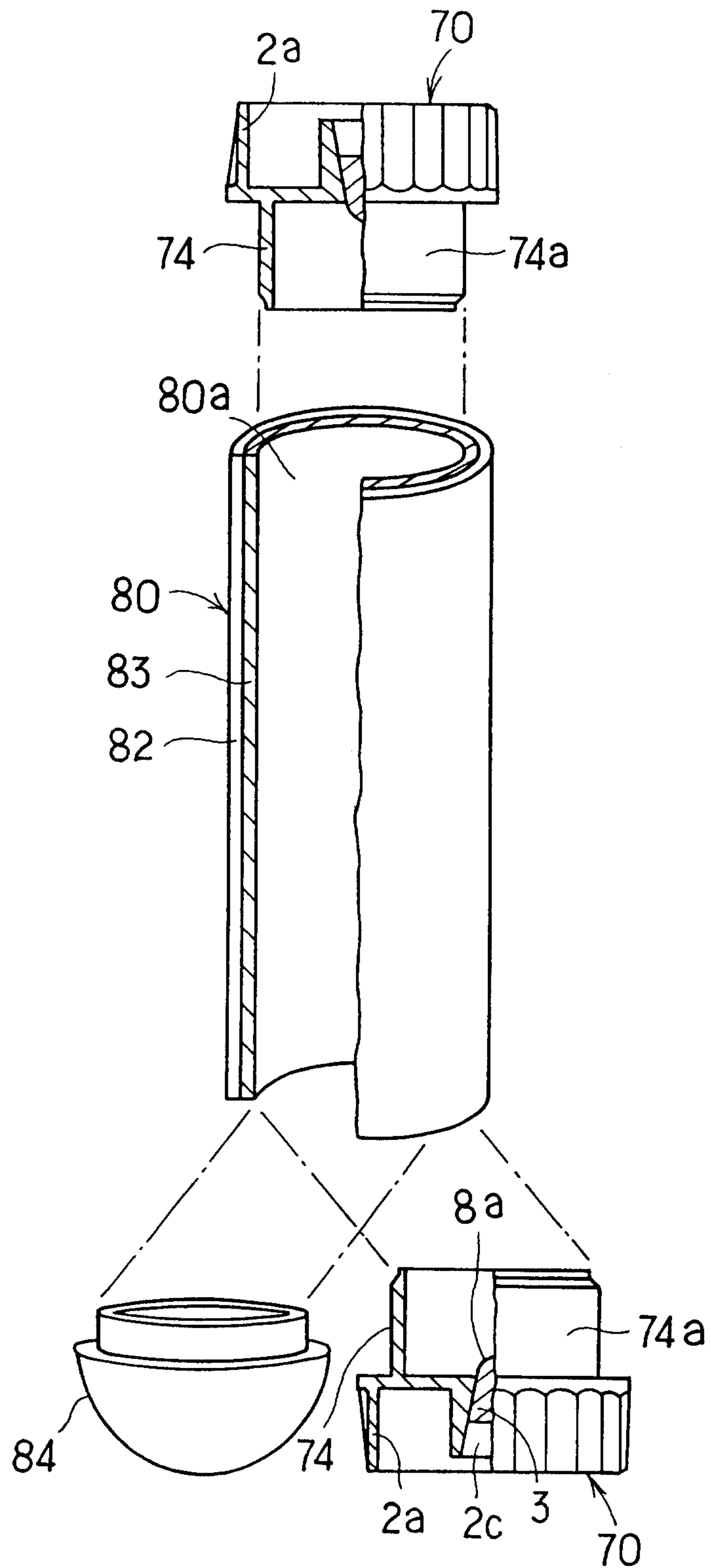
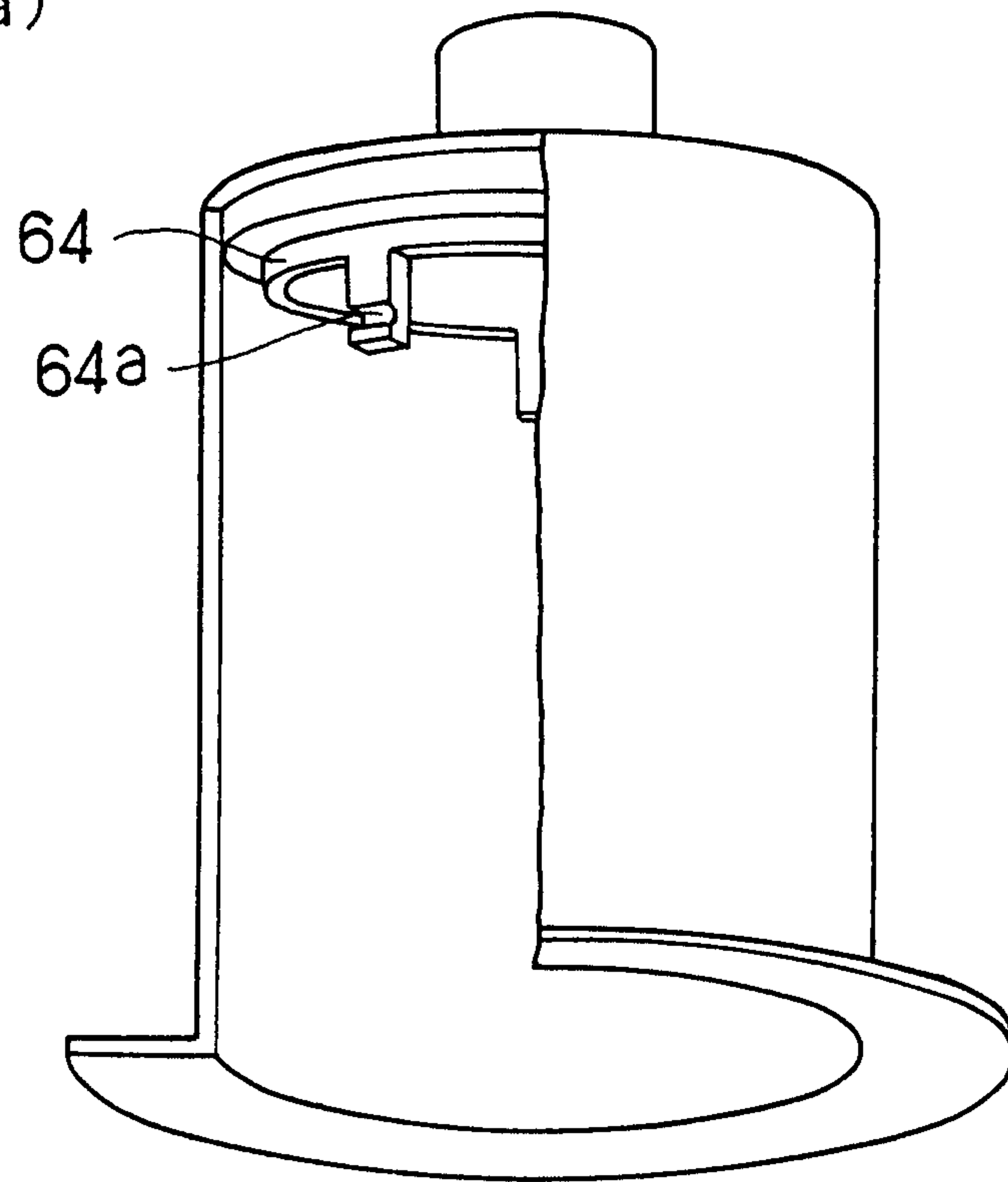


FIG. 16

(a)



(b)

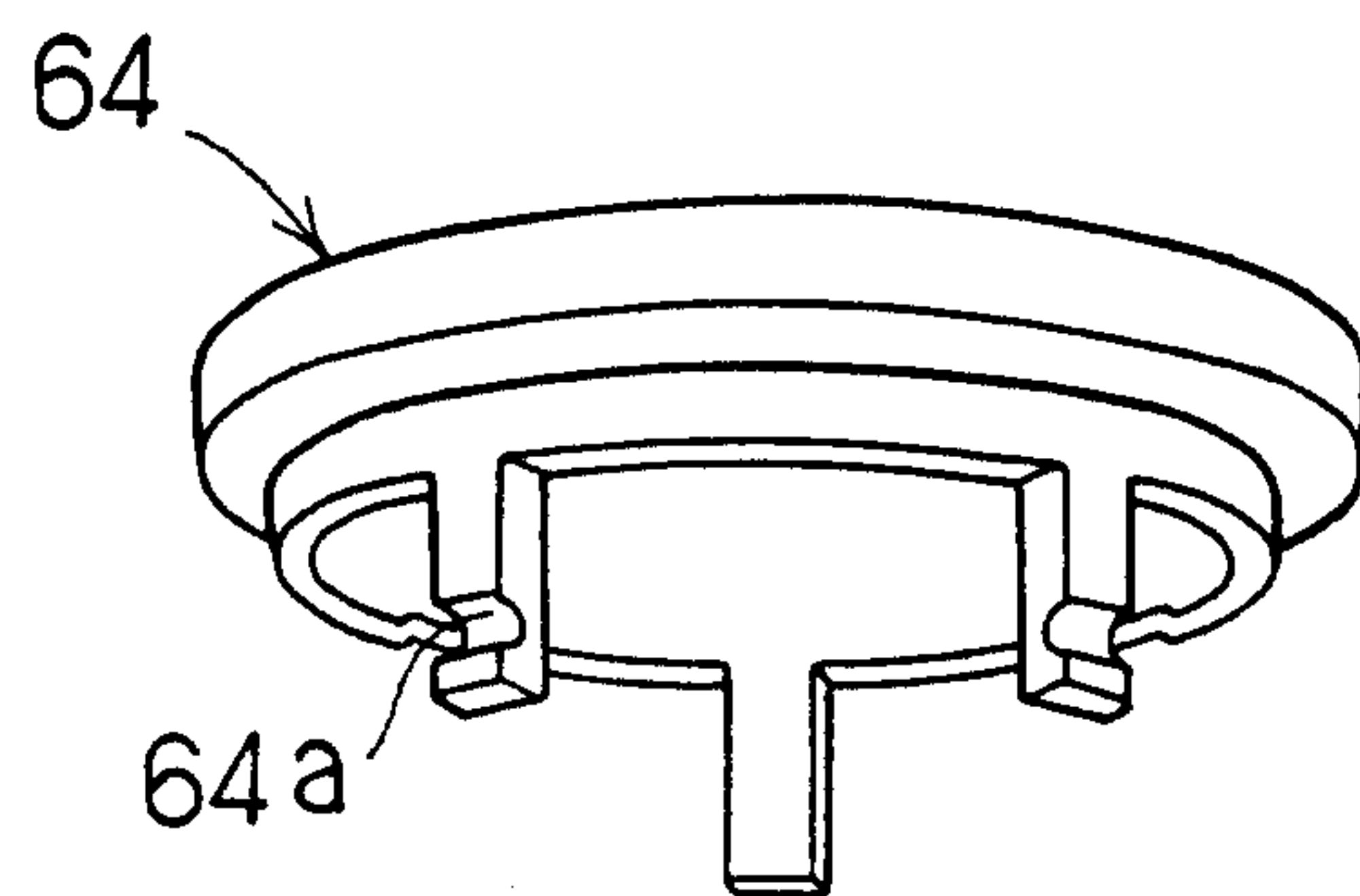


FIG. 17

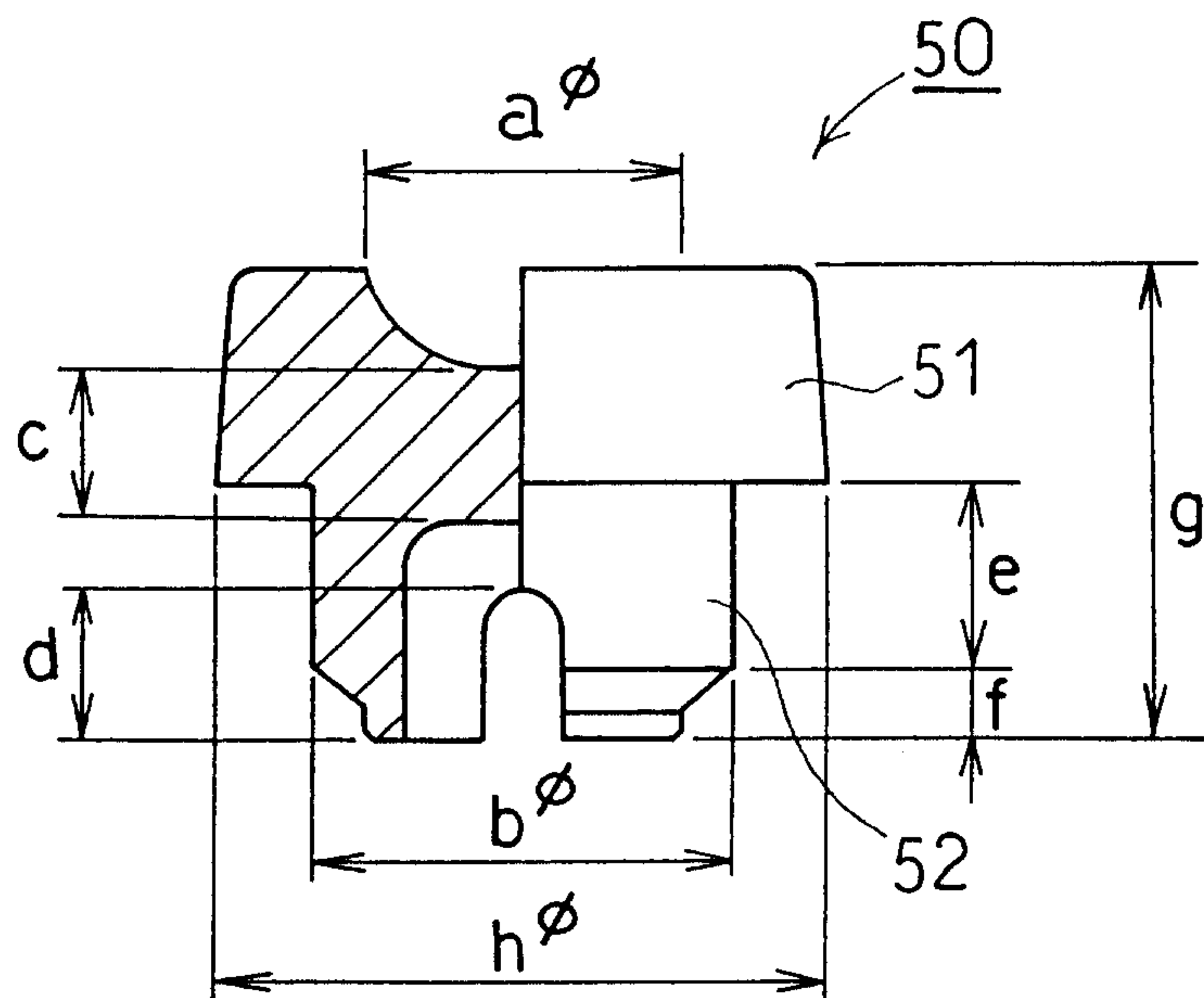


FIG. 18

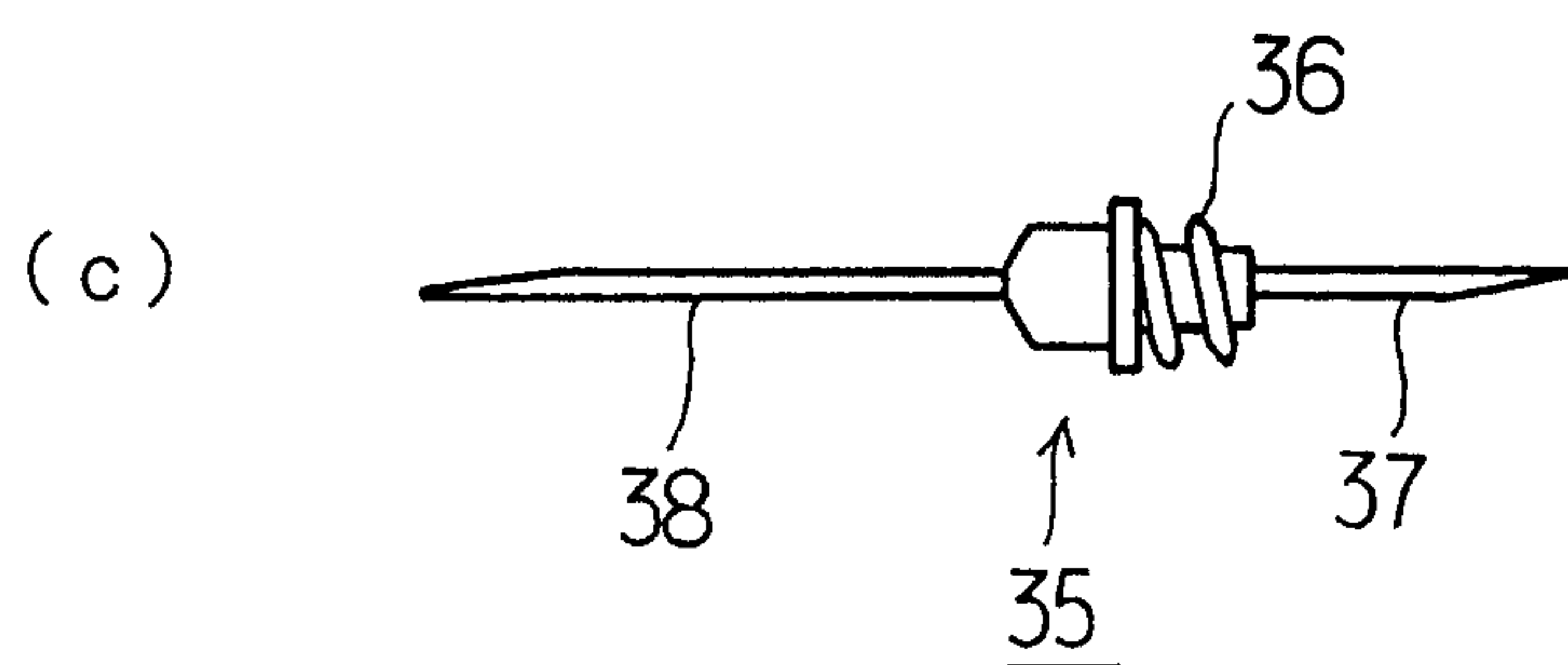
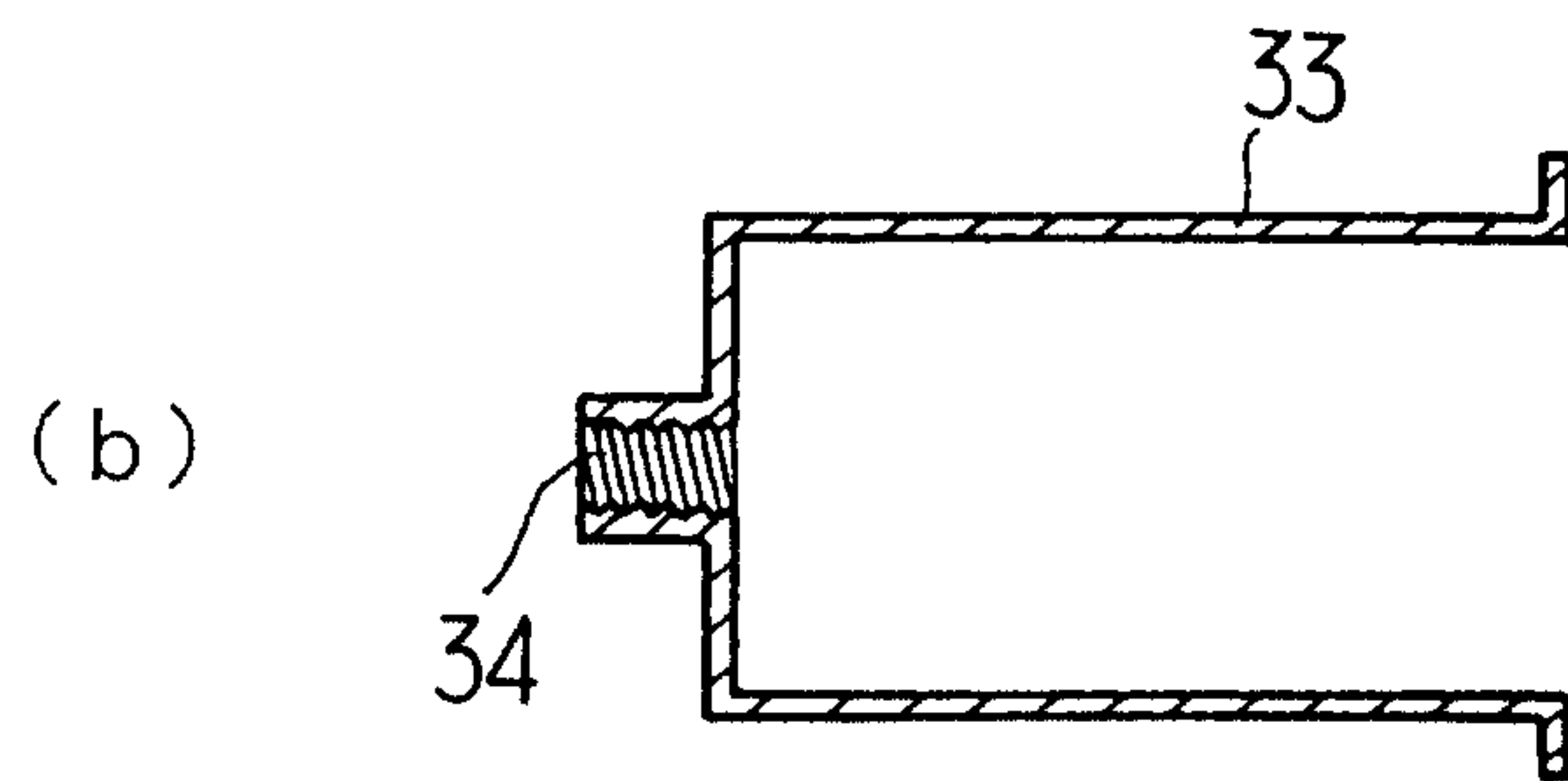
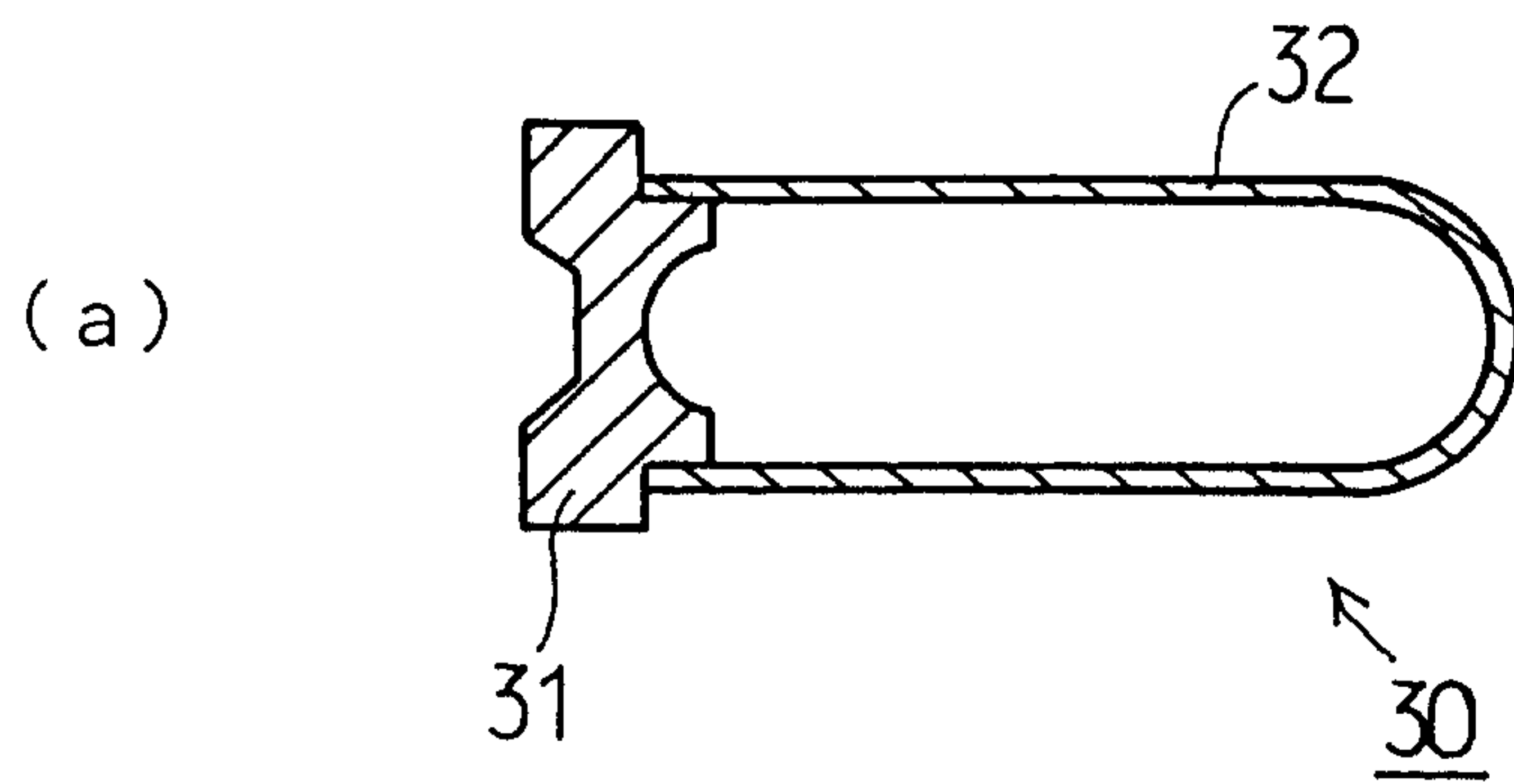


FIG. 19

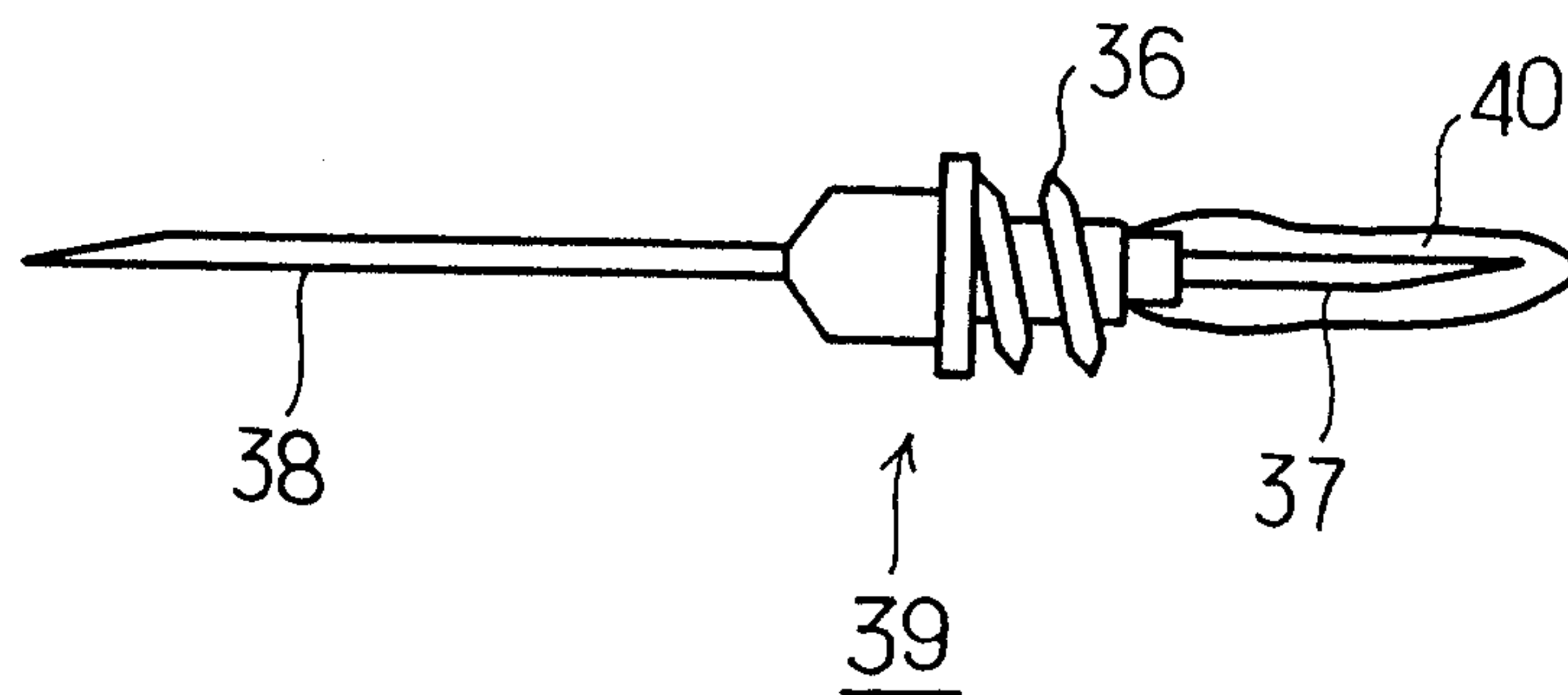


FIG. 20

