A dosage form and a method are disclosed for delivering to a human patient a drug in an ascending amount over time.
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ASCENDING-DOSE DOSAGE FORM

FIELD OF THE INVENTION

This invention relates to a dosage form for delivering an increasing dose of drug. The invention concerns further a dosage form for delivering an increasing dose of drug per unit time over an extended time for continuous effective therapy. The invention pertains additionally to a novel longitudinal dosage form comprising a lengthwise dimension greater than its diameter-wise dimension for delivering an increased dose of drug over a sustained period of therapy. The invention concerns further a method for delivering a dose of drug from the dosage form provided by this invention in an ascending dose for a known therapeutic purpose.

BACKGROUND OF THE INVENTION

For a long time, from antiquity to the present, pharmacy and medicine in all societies used medicines as chemotherapeutics, cancer chemotherapeutics, antiviral therapeutics, for treating neurological maladies, as immunosuppressive drugs, for pain relief, for managing mood, thought, feeling, behavior, psychological personality and pharmacological benefits. The medicines used in these therapies are represented by analgesics, antineoplastics, cytoprotectives, vasomodifiers, opioids, barbiturates, hypnotics, central nervous system stimulants, psychostimulants, psychodepressants, alcohols, cannabinoids, catecholamines, and therapies known in the United States Pharmacopeia, 1997 Ed. While these medicines or therapies have a benefit, a serious problem, called tolerance, is associated with their use. The development of tolerance to a drug results from adaptive changes within the affected patient, such that the therapeutic response is reduced in the presence of the same dose of drug. Tolerance to some drugs, for example, to opioids, is characterized by a shortened duration and decreased intensity of the therapeutic effect. Most of the tolerance seen with
many drugs is due to adaptation of cells in the nervous system to the drug's in
vivo action, as noted in *The Pharmacological Basis of Therapeutics*,

In the broad practice of medicine to which this invention is relevant,
one class of these drugs that has become the standard intervention for the
management of behavior and personality, including attention deficit disorders,
is the central nervous system stimulants. While this invention presents the
central nervous system acting drugs in detail, it is understood the invention is
generic and it embraces drugs broadly as administered by the dosage form,
and the mode and the manner of this invention.

The benefits perceived by health-care providers, physicians,
psychiatrists, psychologists, social workers, and clinicians are dramatic for
central nervous system drugs, and this has resulted in the widespread and
accepted use of the central nervous system acting drugs to treat attention
deficit disorder. In the latest period for collecting data, 1996, it was observed
that about two percent of the school-aged female population and about six
percent of the school-aged male population, for a total of about two million
patients, were administered medication for attention deficit disorder.

Prior to this invention, drugs including opioids, barbiturates, hypnotics,
central nervous system stimulants, central nervous system depressants,
psychostimulants, alcohols, cannabinoids, catecholamines and other drugs
were administered by a standard pharmaceutical dosage form. For example,
one prior art dosage form for administering a drug consists in using an
immediate release tablet containing the drug. This immediate release form
delivers the drug by instant dumping of the drug and produces uneven blood
levels characterized by peaks and valleys. For an immediate-release dosage
form containing a drug that has a rapid onset and a short half-life, this drug
may need multiple doses each day and this can result in swings in blood
levels as the medication loses its therapeutic effect. This type of dosage
form does not provide the needed therapy over an extended time.
Another prior art dosage form for dispensing a drug is the sustained-release dosage form. The sustained-release dosage form delivers a drug in a nonascending profile, often in a descending profile, over time. This dosage form, however, may not provide the required therapy and the appropriate blood pattern. For drugs, such as the central nervous system acting drugs, that are delivered from a sustained-release, nonascending dosage form, the patient often develops an acute tolerance to the drug which is manifested by a short duration and a decrease in the intensity needed for acceptable therapy. The prior art sustained-release dosage form is devoid of means that compensate for its shortcomings inherent therein.

The above presentation teaches that a critical and pressing need exists for a novel dosage form for delivering a drug that overcomes the shortcomings known to the prior art. That is, a long-felt need exists for a dosage form for (1) delivering a drug in a sustained-ascending rate that simultaneously reduces or eliminates the need for frequency of daily dosing; for (2) delivering a drug in a sustained-compensating dose to substantially compensate for acute tolerance to the drug and thereby maintain a preselected clinical profile; for (3) administering the drug in an increasing dose to lessen or eliminate acute or chronic tolerance to the drug to provide effective therapy; and (4) for delivering the drug in a sustained, ascending-controlled profile clinically indicated for both medical and psychomedical effects.

OBJECTS OF THE INVENTION

Accordingly, in view of the above presentation, it is an immediate object of this invention to provide a novel and unique dosage form that overcomes the shortcomings known to the prior art and thereby makes an advancement in the drug dispensing art.
Another object of the invention is to make available to the medical and mental health arts a novel and unique dosage form that provides an ascending dose of drug over a sustained time.

Another object of the invention is to provide a dosage form for maintaining the therapeutic effect of a drug in a patient that acquires a tolerance to the drug, wherein the dosage form comprises a dose of drug that is released in an ascending dose to a patient that acquired tolerance to the drug to lessen the effect of tolerance and concomitantly provide the intended therapy.

Another object of the invention is to provide a dosage form for maintaining the therapeutic effect of a drug in a patient that acquired acute tolerance to the drug, wherein the dosage form is designed and shaped as a tablet for oral administration and delivers to a patient the drug in a dosage form controlled, increasing dose to compensate for the acute tolerance associated with this drug.

Another object of the invention is to provide a dosage form designed and shaped as an osmotic tablet for oral administration into the gastrointestinal tract, comprising a dose of drug for administering to a patient that acquires chronic tolerance to the drug, for administering the drug in a controlled increasing dose, to provide drug compensation for the acquired chronic tolerance associated with the drug.

Another object of the invention is to make available a dosage form comprising a length greater than its thickness for lessening the incidence of acquired tolerance in a patient, wherein the dosage form is characterized by administering the drug in a sustained and increasing dose over time to produce the intended therapeutic effect.

Another object of the invention is to provide a dosage form manufactured as a longitudinal tablet possessing a lengthwise dimension in excess of its diameter-wise dimension for administering a drug selected from the group consisting of an opioid, barbiturate, hypnotic, central nervous system stimulant, central nervous system depressant, psychostimulant,
cannabinoid and catecholamine in a controlled, changing dose that
overcomes the shortcomings known to the prior art.

Another object of the invention is to make available a method for
lessening the incidence of acquired tolerance in a patient administered a
drug that develops tolerance in the patient, wherein the method comprises
an improvement by administering a dosage form manufactured initially as a
compressed tablet that in operation in a fluid environment dispenses a drug
in a sustained and increasing dose to substantially lessen the unwanted
effects of tolerance and to produce the intended therapy over four hours to
thirty hours.

Another object of the invention is to make available a dosage form,
designed as an oral pharmaceutically acceptable tablet, comprising a first
layer of drug and a second layer that pushes the first layer from the tablet,
to provide a sustained and ascending dose of drug.

Another object of the present invention is to make available a method
for administering a drug in a sustained and increasing dose by administering
an osmotic dosage tablet comprising a drug composition that delivers the
drug in an initial concentration, followed by a second, higher concentration
from the original drug composition to effect a sustained and ascending dose
of drug.

Another object of the invention is to make available a dosage form
manufactured as an osmotic tablet comprising a single composition
containing a drug administered in a sustained and ascending dose profile
over time.

Another object of the invention is to make available a dosage form
manufactured as an osmotic tablet comprising an immediate-release dose of
drug on the exterior of the osmotic tablet, and a prolonged-ascending dose in
the interior of the osmotic tablet, which exterior and interior doses operate
successively to provide an ascending dose of drug to negate acquired and
developed tolerance.
Another object of this invention is to make available a dosage form manufactured as an osmotic oral tablet comprising an immediate dose of drug on the exterior of the osmotic tablet, and an interior bilaminate comprising a drug laminate comprising a dose of drug, and an expandable laminate comprising an expandable hydrogel, which osmotic tablet in operation delivers a dose of drug immediately in up to one hour from the exterior of the osmotic tablet, and a dose of drug in from fifteen minutes up to twenty-four hours from the interior of the osmotic tablet by the expandable laminate pushing the interior drug from the osmotic tablet, whereby through the combined operations of the exterior dose, the interior laminate, and the expandable laminate, the osmotic tablet provides an ascending dose of drug for therapy over time.

These objects, as well as other objects, features and advantages of this invention will become more apparent from the following detailed disclosure of the invention accompanied by the accompanying claims.

**BRIEF DESCRIPTION OF THE DRAWING FIGURES**

Figure 1 illustrates an ascending release rate profile for a dosage form comprising the drug pseudoephedrine hydrochloride as provided by the invention;

Figure 2 depicts an ascending-increasing dose release rate for a dosage form of the invention comprising the central nervous system stimulating drug methylphenidate hydrochloride; and,

Figure 3, depicts the release rate in mg/hr for methylphenidate from a dosage form provided by the invention.

**DETAILED DESCRIPTION OF SPECIFICATION**

In accordance with the practice of this invention, it has now been discovered a novel dosage form can be made available characterized by an
ascending rate of drug delivery over time. The dosage form provided by this
invention delivers a drug at a continuously increasing rate for a predetermined
period of time. The dosage form of this invention is unexpected and it is a
breakaway from the prior art existing dosage form technologies that deliver
a drug at a constant zero-order unchanging rate over time. The dosage form
of this invention avoids delivery at a zero order rate as it delivers a drug
continuously in an ascending rate over time. The profile of the prior art
dosage form consists of a short start-up in delivery, followed by a constant
unchanged rate. The profile of this invention departs from the prior art by
making available a dosage form wherein the drug release rate follows an
ascending profile to achieve a desired drug delivery pattern. The dosage
form of this invention achieves the ascending pattern by combining the
dimensions of the dosage form with the internal formulation of the dosage
form.

The dosage form of this invention comprises a wall that surrounds
an internal compartment. The wall of the dosage form comprises a
semipermeable composition permeable to the passage of fluid present in
an environment of use, such as the aqueous biological fluid of the
gastrointestinal tract, and the wall is impermeable to the passage of drug.
The wall maintains its physical and chemical integrity during the drug
dispensing life of the dosage form. The semipermeable wall comprises a
polymer selected from the poly(cellulose) group consisting of cellulose
acrylate, cellulose diacylate, cellulose triacylate, cellulose acetate, cellulose
diacetate and cellulose triacetate. The wall comprises 100 wt% (weight
percent) of said poly(cellulosic) polymer possessing a number-average
molecular weight of 15,000 to 4,000,000. The wall, in another manufacture,
can comprise from 40 wt% to 100 wt% of the poly(cellulosic) polymer and
from 0 to 35 wt% of a hydroxypropylalkylcellulose selected from the group
consisting of hydroxypropylmethylcellulose, hydroxypropylethylcellulose,
hydroxypropylbutylcellulose, and hydroxypropylpentylcellulose of 9,000 to
240,000 number-average molecular weight; 0 to 25 wt% of a
hydroxyalkylcellulose comprising a member selected from the group
consisting of hydroxymethylcellulose, hydroxyethylcellulose,
hydroxypropylcellulose, and hydroxybutylcellulose of 7,500 to 200,000
number-average molecular weight; and 0 to 25 wt% of poly(ethylene glycol)
of 190 to 40,000 intrinsic viscosity molecular weight. The total weight of all
components comprising the wall is equal to 100 wt%. Wall-forming polymers
are known in U.S. Patent Nos. 3,845,770; 3,916,899; 4,036,228; 4,111,202;
and 5,178,866.

The dosage form comprises one or more than one exit in the wall that
connects the exterior of the dosage form with the interior of the dosage form.
The term "exit" as used herein comprises a passageway, orifice, pore,
micropore, micro-opening, hollow fiber, capillary tube, porous overlay, porous
insert, and osmotic opening for dispensing a drug from the dosage form.
The exit passageway embraces further a material that erodes, or is leached
from the wall in a fluid environment of use, such as the gastrointestinal tract.
Representative materials for forming an erodible passageway include erodible
poly(glycolic) acid, erodible poly(lactic acid), erodible poly(orthoester),
erodible poly(orthocarbonate), erodible poly(acetal), a gelatinous filament,
poly(vinyl alcohol), leachable materials including fluid removable pore-forming
polysaccharides, salts, sugars and oxides. An exit can be formed by leaching
compounds such as sorbitol, lactose or glucose. The exit can have any
operative shape such as round, triangular, square, or elliptical. The dosage
form can be provided with one or more passageways close together or in
spaced apart positions on a common surface of the dosage form.
Passageways and equipment for forming an exit are disclosed in U.S.
Patent Nos. 3,845,770; 3,916,899; 4,063,064; 4,088,864; 4,200,098;
4,285,987; and 5,178,866.

The dosage form comprises internally a first drug layer and a second
expandable layer. The first layer is next to the exit to provide for drug delivery
from the dosage form. The first layer comprises a dose of 240 ng
(nanograms) to 700 mg (milligrams) of drug, and from 1 mg to 200 mg of a
pharmaceutically acceptable carrier. The pharmaceutically acceptable carrier comprises a hydrophilic polymer selected from the group consisting of a poly(alkylene oxide) of 25,000 to 1,000,000 number-average molecular weight where a 5% aqueous solution exhibits a viscosity at 25°C of 12 to 17,600 cps (centipoise) represented by a member selected from the group consisting of poly(methylene oxide), poly(ethylene oxide), poly(propylene oxide), poly(butylene oxide), copolymer poly(ethylene oxide)-poly(propylene oxide); and a blend of two different poly(alkylene oxides), such as a poly(alkylene oxide) of 40,000 to 500,000 molecular weight with a different poly(alkylene oxide) of 40,000 to 500,000 molecular weight, a poly(ethylene oxide) of 100,000 molecular weight with a poly(ethylene oxide) of 200,000 molecular weight, or a poly(ethylene oxide) of 200,000 molecular weight with a poly(ethylene oxide) of 300,000 molecular weight, which poly(alkylene oxide) polymers are available from Union Carbide Corp.; 0 mg to 200 mg of a pharmaceutical excipient such as starch, talc, mannitol, sorbitol, glucose, fructose, polysaccharides or silicon dioxide; 0 mg to 125 mg of a hydrophilic pharmaceutically acceptable carboxyvinyl polymer, also known as carboxypolyalkylene polymer, possessing a 7,500 to 1,000,000 number-average molecular weight, including a carboxyvinyl polymer of 450,000 number-average molecular weight, a carboxyvinyl polymer of 750,000 number-average molecular weight, a carboxyvinyl polymer of 1,250,000 number-average molecular weight, and a carboxyvinyl polymer of 3,000,000 number-average molecular weight, as disclosed in U.S. Patent Nos. 2,798,053; 2,909,462; and 3,825,068, and available as Carbopol® polymer from B.F. Goodrich Company; and 0 mg to 250 mg of a pharmaceutically acceptable alkali carboxymethylcellulose, wherein the alkali is sodium or potassium represented by sodium carboxymethylcellulose of 10,000 to 7,000,000 viscosity-average number molecular weight, available from the Hercules Corporation; a surfactant selected from 0.0 mg to 7.5 mg of a member selected from the group consisting of amphoteric, anionic, cationic, and nonionic surfactants, as represented by sorbitan trioleate,
sorbitan tristearate, ethylene glycol fatty acid ester, polyethylene glycol monostearate, sorbitan sesquioleate, glycerol monostearate, sorbitan monooleate, propylene glycol monolaurate, sorbitan monostearate, diethylene glycol monolaurate, sorbitan monopalmitate, polyoxyethylene mannitol dioleate, sorbitan monolaurate, polyoxyethylene lauryl ether, polyoxyethylene monostearate, polyethylene glycol 400 monostearate, triethanolamine oleate, polyoxyethylene alkyl phenol, polyethylene alkyl aryl ether, polyoxyethylene sorbitan monolaurate, polyoxyethylene sorbitan monopalmitate, polyoxyethylene monostearate, polyoxyethylene sorbitan monolaurate, polyoxyethylene lauryl ether, sodium oleate, and sodium lauryl sulfate, which surfactants are known in Pharmaceutical Sciences, Remington, 17th Ed., pp. 1305-1306 (1985); 0 mg to 20 mg of a hydroxypropylalkylcellulose binder selected from the group consisting of hydroxypropylmethylcellulose, hydroxypropylethylcellulose, hydroxypropylbutylcellulose and hydroxypropylpentylcellulose of 9,000 to 750,000 number-average molecular weight, available from the Dow Chemical Company, and a polyvinylpyrrolidone binder of 7,500 to 350,000 molecular weight; and 0.0 mg to 20 mg of a hydroxyalkylcellulose selected from the group consisting of hydroxymethylcellulose, hydroxyethylcellulose, hydroxypropylcellulose, hydroxybutylcellulose and hydroxypentylcellulose of 7,500 to 750,000 weight-average molecular weight, available from Aqualon Company; and 0.01 mg to 5 mg of a lubricant such as stearic acid, magnesium stearate, calcium stearate, potassium oleate, magnesium laureate and calcium palmitate. The expression "pharmaceutically acceptable" as used herein means the polymer, compound or drug denotes nontoxic and is acceptable for oral administration to a human patient.

The dosage form comprises a second layer that displaces or pushes the first drug layer through the exit port from the dosage form. The second layer comprises 100 ng to 400 mg of a hydrophilic osmopolymer selected from the group consisting of a poly(alkylene oxide) of 1,500,000 to
10,000,000 number-average molecular weight; or an alkali
carboxyalkylcellulose of 1,750,000 to 10,000,000 of viscosity-average
number molecular weight; 0 to 100 mg of a hydroxypropylalkylcellulose
comprising hydroxypropylmethylcellulose, hydroxypropylethylcellulose,
hydroxypropylbutylcellulose and hydroxypropylpentylcellulose of 9,000 to
750,000 number-average molecular weight; 0 to 400 mg, generally 25 mg
to 400 mg, of a hydroxyalkylcellulose selected from hydroxymethylcellulose,
hydroxyethylcellulose, hydroxypropylcellulose and hydroxybutylcellulose of
7,500 to 1,500,000 number-average molecular weight; from 0 to 250 mg,
with a present manufacture of 10 mg to 175 mg, of an osmagent, also known
as osmotically effective solute, osmotically effective compound, and osmotic
agent, including inorganic and organic compounds, selected from the group
consisting of magnesium sulfate, magnesium chloride, sodium chloride,
lithium chloride, potassium sulfate, sodium sulfate, lithium sulfate, potassium
chloride, sodium sulfate, magnesium succinate, tartaric acid; carbohydrates
such as raffinose, sucrose, glucose and lactose; from 0.001 mg to 10 mg of a
surfactant selected from the group consisting of amphoteric, anionic, cationic
and nonionic surfactants, present in the first drug layer; 0 mg to 20 mg of a
carboxyvinylpolymer of 7,500 to 10,000 number-average molecular weight,
present in the first drug layer; 0 mg to 5 mg of a colorant compound to identify
the dosage form, such as red ferric oxide or black ferric oxide; and 0 mg to
5 mg of a lubricant including the lubricants presented in the first drug layer.

The dosage form provided by this invention is designed and shaped
as a dosage form tablet. The dosage form tablet comprises a length greater
than its width individually. The dosage form tablet comprises a length of
5 mm to 28 mm, and a width of 2.50 mm to 10 mm. The dosage form tablet
provided by this invention comprises in the second layer 60% to 95% of
osmopolymer, or 60% to 95% of a combination comprising an osmopolymer
and an osmagent. The high percent of osmopolymer, or high percent
osmopolymer and osmagent composition, joined with the dimensions of the
dosage form tablet, enables the dosage form tablet to make available an
ascending delivery of drug for 2 hours to 24 hours.

Representative of a drug present in the drug layer comprises a drug
composition comprising an opioid, barbiturate, hypnotic, central nervous
system acting drug, psychostimulant, psychodepressant, analgesic, alcohol,
cannabinoid, and catecholamine. Examples of drugs are central nervous
system acting drugs for the management of attention deficit disorder,
including catecholamines and drugs that can mimic their action. The drugs
for this therapy comprise a member selected from the group consisting of
amphetamine, dextroamphetamine, methamphetamine, methylphenidate,
racemic methylphenidate, threomethylphenidate, ethylphenidate,
phenylisopropylamine and pemoline. The drugs include racemates,
stereoisomers and enantiomers of a racemic drug. The drugs include their
pharmaceutically acceptable salts, such as a member selected from the
group consisting of hydrochloride, fumarate, sulfate, phosphate, lactate,
malate, acetate, tartrate, hydrobromide, citrate, pamoate, maleate, ascorbate,
gluconate, aspartate, and salicylate.

The invention comprises further, on the external surface of the dosage
form, a coat composition comprising a drug. The coat composition is an
external overcoat carried by the dosage form. The external overcoat on the
wall of the dosage form comprises a dose of drug, and the overcoat
cooperates with the interior compartment comprising a dose of drug that
delivers the drug, to provide an initial unexpected ascending drug delivery
profile. The overcoat provides an initial dose of drug followed by a dose of
drug from the interior of the dosage form to give an ascending drug delivery
profile. The overcoat comprises 10 ng to 100 mg of a drug that is delivered in
up to one hour, followed by the dose from the dosage form. The dose of drug
from the interior is delivered over 24 hours. The overcoat comprises a drug
selected from the group consisting of opioids, barbiturates, hypnotics,
psychostimulants, psychodepressants, central nervous system acting drugs,
analgesics and catecholamines. Representative of individual drugs present in
the overcoat comprise a drug selected from the group consisting of
ampheta mine, dextroamphetamine, methamphetamine, methylphenidate,
racemic methylphenidate, threomethylphenidate, ethylphenidate,
alkylphenidate, phenylisopropylamine, and pemoline. These drugs include
their pharmaceutically acceptable salts such as a member selected from the
group consisting of hydrochloride, sulfate, phosphate, acetate, hydrobromide,
pamoate, maleate, maleate, fumarate, ascorb ate, tartrate and citrate.
Representative of a drug embodiment present in the overcoat is an
alkylphenidate comprising 10 ng to 25 mg of methylphenidate.

The overcoat comprises the drug blended with a pharmaceutically
acceptable carrier. The pharmaceutically acceptable carrier comprises an
aqueous, drug-releasing carrier selected from the group consisting of an
alkylcellulose, methylcellulose, ethylcellulose, hydroxyethylcellulose,
hydroxymethylcellulose, hydroxypropylcellulose, hydroxyethylcellulose,
hydroxybutylcellulose, hydroxypropylalkylcellulose,
hydroxypropylmethylcellulose, hydroxypropylethylcellulose,
hydroxypropylbutylcellulose, methyl dextrose, acacia, guar gum,
pregelatinized starch, propylene glycol alginate and cyclodextrin.
The overcoat comprises 0.01 wt% to 15 wt% of the pharmaceutically
acceptable carrier. The dosage form overcoat in another manufacture
comprises 0.01 wt% to 5 wt% of a member selected from the group
consisting of polyethylene glycol, polypropylene glycol, polyvinylpyrrolidone,
and acetylated triglycerides. The overcoat provides needed drug therapy,
for example, methylphenidate, as the overcoat dissolves or undergoes
dissolution in the presence of fluid present in the gastrointestinal tract of a
patient. Thus, the overcoat provides drug therapy on oral administration into
the patient's drug receiving environment, the gastrointestinal tract, for an
immediate therapeutic benefit.

The wall of the dosage form in one manufacture is formed by an air-
suspension procedure. This procedure consists of suspending and tumbling
compressed bilayer cores in a current of air and wall-forming composition until
a wall is applied forming and surrounding an internal compartment containing
the bilayer core. The air-suspension procedure is well suited for forming the
wall. The air-suspension procedure is described in U.S. Patent Nos.
2,799,241 and 5,082,668. The wall can be formed in an air-suspension
coater using cosolvents. Representative cosolvents are: methylene
dichloride-methanol, 80:20 wt:wt; or acetone-water cosolvent 85:15, or 90:10,
or 95:5, or 99:1 wt:wt, using 1% to 7% solids. Other wall-forming techniques
can be used, such as a pan coating system, or a wall forming composition
deposited by successive spraying of the composition accompanied by
tumbling in a rotating pan. A pan coater may be used to produce thicker
walls. A large volume of solvent can be used in a solvent system to produce
a thinner wall. Finally, the wall-coated compartment is dried in an oven at
30°C to 50°C for up to a week, or in a humidity controlled oven at 50 RH
(relative humidity) and 50°C for 18 hours to 3 days.

The first and second layers of the invention are made by standard
manufacturing techniques. For example, in one manufacture the drug and
other ingredients are blended and pressed into a solid layer. The drug and
the ingredients can be blended with a solvent and mixed into a semisolid or
solid formed by conventional methods such as ball-milling, calendering,
stirring or roller milling, and then pressed into a preselected shape. The first
layer possesses dimensions that correspond to the internal dimensions of the
area the layer occupies in the dosage form. It also possesses dimensions
concerning the second layer for forming a contacting bilayer
arrangement therewith. The push layer comprising the osmopolymer, or
osmopolymer and osmagent, is placed in contact with the first drug layer.
The push layer, a displacement layer for displacing the drug layer from the
dosage form, is manufactured using the techniques for providing the first drug
layer. The layering of the first drug layer and the second displacement layer
can be fabricated by conventional press layering techniques. The bilayered
compartment-forming core is surrounded and coated with an outer wall
comprising a semipermeable composition. An exit is laser drilled through the
wall to contact the first drug layer. The dosage form is optically oriented automatically by the laser equipment for forming the exit passageway.

In another manufacture, the dosage form is manufactured by the wet granulation technique. In the wet granulation technique, for example, the drug and the ingredients comprising a drug layer are blended using an organic solvent, such as isopropyl alcohol-methylene dichloride 80:20 v:v (volume:volume), or methanol-methylene dichloride, as the granulation fluid. Other granulating fluid, such as denatured alcohol 100%, can be used for this purpose. The ingredients forming the drug layer are individually passed through a screen and then thoroughly blended in a mixer. Next, other ingredients comprising the drug layer are dissolved in a portion of the granulation fluid, such as the solvents described above. Then, the latter prepared wet blend is slowly added to the drug blend with continual mixing in the blender. The granulating fluid is added until a wet blend is produced, which wet mass is forced through a screen onto oven trays. The blend is dried for 7 to 24 hours at 30°C to 50°C. The dry granules are then sized with a screen. Next, a lubricant is passed through a screen and added to the dry screen granule blend. The granulation is put into milling jars and mixed on a jar mill for 1 to 15 minutes. The other drug layer and the displacement layers are made by the same wet granulation techniques. The compositions are pressed into their individual layers in standard presses, such as a layer press.

Another manufacturing process that can be used for providing the compartment-forming compositional layers comprises blending the powdered ingredients for each layer independently in a fluid bed granulator. After the powdered ingredients are dry blended in the granulator, a granulating fluid, for example, poly(vinylpyrrolidone) in water, or in denatured alcohol, or in 95:5 ethyl alcohol/water, or blends of ethanol and water, is sprayed onto the powders. Optionally, the ingredients can be dissolved or suspended in the granulating fluid. The coated powders are then dried in a granulator. This process granulates all the ingredients present therein while adding the granulating fluid. After the granules are dried, a lubricant, such as stearic
acid, calcium stearate, magnesium oleate, potassium oleate, or magnesium stearate, is added to the granulator. The granules for each separate layer are then pressed in the manner described above.

The dosage form of this invention is manufactured in another manufacture by first mixing a known dose of drug with compositional layer-forming ingredients, and then pressing under one-eighth to three tons the composition into a solid layer possessing dimensions that correspond to the internal dimensions of the compartment of the dosage form. The contacting second layer, comprising an osmopolymer, or an osmopolymer and an osmagent, is manufactured in a like manner. In another manufacture, the first and second layers independently are manufactured by mixing the drug and composition forming ingredients and a solvent into a solid, or into a semisolid, by conventional methods such as ball milling, calendering, stirring or roller milling, and pressed into a layer. Next, the first layer is placed next to a layer of a displacement composition comprising an osmopolymer and an optional osmagent. Then, the two-layered core is surrounded with a semipermeable wall. The layering of the first layer and the second layer can be accomplished by layer tablet press technique and longitudinal compressed tablet technique. A wall can be applied by molding, spraying or dipping the pressed-shape bilayered core into wall forming materials. Another technique that can be used for applying the wall is the air-suspension coating procedure. This procedure consists in suspending and tumbling the two-layered laminate in a current of air until the wall forming composition surrounds the bilayer.


Exemplary solvents suitable for manufacturing the wall, the layer and the wall include inert inorganic and organic solvents. The solvents broadly
include members selected from the group consisting of aqueous solvents, alcohols, ketones, esters, ethers, aliphatic hydrocarbons, halogenated solvents, cycloaliphatics, aromatics, heterocyclic solvents and mixtures thereof. Typical solvents include acetone, diacetone alcohol, methanol, ethanol, isopropyl alcohol, butyl alcohol, methyl acetate, ethyl acetate, isopropyl acetate, n-butyl acetate, methyl isobutyl ketone, methyl propyl ketone, n-hexane, n-heptane ethylene glycol monoethyl ether, ethylene glycol monoethyl acetate, methylene dichloride, ethylene dichloride, propylene dichloride, carbon tetrachloride, chloroform, nitroethane, nitropropane, tetrachloroethane, ethyl ether, isopropyl ether, cyclohexane, cyclooctane, benzene, toluene, naphtha, tetrahydrofuran, diglyme, aqueous and nonaqueous mixtures thereof, such as acetone and water, acetone and methanol, acetone and ethyl alcohol, methylene dichloride and methanol, ethylene dichloride and methanol, and methylene dichloride and ethanol.

The solvents are disclosed in U.S. Patent No. 5,030,456.

DETAILED DESCRIPTION OF THE EXAMPLES

The following examples are illustrative of the present invention, and the examples should not be considered as limiting the scope of the invention in any way, as these examples, and other equivalents thereof, will become apparent to those versed in the art in the light of the present disclosure and the accompanying claims.

EXAMPLE 1

An osmotic dosage form designed and shaped to deliver a drug that stimulates the central nervous system by administering a drug in an ascending release profile is manufactured as follows: First, a binder solution is prepared as follows: 300 g of poly(vinylpyrrolidone) having a number-average molecular weight of 40,000 is added to a mixing vessel containing
2700 g of distilled water. The mixture is stirred until the poly(vinylpyrrolidone) dissolved in the water and produces a clear solution. Next, a drug formulation is prepared as follows: 6,564 g of poly(ethylene oxide) having a number-average molecular weight of 200,000 is passed through a 40 mesh screen. Then, 3,282 g of the screened poly(ethylene oxide) is placed into the bowl of a fluid bed granulator. Next, 1,024 g of central nervous system acting methylphenidate hydrochloride is placed into the granulator with the poly(ethylene oxide). Then, 100 g poly(vinylpyrrolidone) of number-average molecular weight 40,000 is added to the granulator; then the remaining 3,182 g of poly(ethylene oxide) is added to the granulator. The addition of the dry ingredients into the bowl is performed so that the methylphenidate hydrochloride is located between two layers of poly(ethylene oxide). The granulation is started with the ingredients inside the bowl fluidized for 2 minutes to obtain a uniform mixing of the powders. Next, the binder solution is sprayed onto the powder bed through nozzles at a spray rate of 100 g/min. During the spraying process, the airflow is maintained at 500 cfm and the temperature kept at 25°C. During the spraying operation, the solution is sprayed for 30 seconds, followed by a shaking time of 10 seconds during which time the powders adhering to the filterbags are dislodged into the granulating chamber. At the end of the spraying operation, the granules are dried in the granulating chamber for an additional 5 to 10 minutes to obtain dry granulation. The methylphenidate hydrochloride granules are passed through a fluid air mill with a 7 mesh screen for size reduction. The screen is U.S. Sieve Series as disclosed in Chemical Engineer's Handbook, Perry, 6th Ed., pp. 21-15 (1984). Next, the screened granules are placed in a blender to which 8 g of magnesium stearate (screened through a 40 mesh screen) and 4 g of powdered butylated hydroxy toluene (screened through a 60 mesh screen) is added to the granules and mixed together.

Next, the displacement or push composition is prepared as follows:
First a binder solution is prepared by adding 937.5 g of poly(vinylpyrrolidone) of 40,000 number-average molecular weight to 8437.5 g of distilled water.
This mixture is stirred until the poly(vinylpyrrolidone) dissolves in water to yield a clear solution. Next, displacement osmotic granules are prepared as follows: First, 13452.5 g of poly(ethylene oxide) having a number-average molecular weight of 7,000,000 is placed into the bowl of a fluid bed granulator. Next, 312.5 g of poly(vinylpyrrolidone) of 40,000 number-average molecular weight is added to the bowl. Then, 10,000 g of osmagent sodium chloride and 250 g of red ferric oxide, which have been milled using a 21 mesh screen, are placed into the bowl. The bowl is attached to the main body of the granulator and the granulation is initiated. Initially, the powder bed inside the bowl is fluidized for 3 minutes to obtain uniform mixing of the powders. Then, the binder solution is sprayed onto the powder bed and the binder solution sprayed thereon at a rate of 240 g/min. During the spraying, the air flow is maintained at 1000 cfm and the temperature kept at 25°C. The solution is sprayed for 30 seconds, followed by shaking for 10 seconds, during which time the powders adhering to the filterbags can be dislodged into the granulating chamber. At the end of the spraying operation, the granules are dried in the granulating chamber for an additional 10 to 15 minutes to obtain dry granulation. The granules are then passed through an air mill with a 7 mesh screen for size reduction. The granules are then transferred to a blender, and 25 g of magnesium stearate (screened through a 40 mesh screen) and 12.5 g of butylated hydroxy toluene (screened through a 60 mesh screen) are added to the granules and mixed together.

Next, the drug composition comprising the methylphenidate and the displacement osmotic composition are compressed together using an automated tablet compression machine capable of compressing the two layers longitudinally together. First, 110 mg of the methylphenidate composition forming layer is added to the die cavity of 4.7 mm diameter, tamped, and then 132 mg of the displacement osmotic composition is placed into the die and compressed together using 0.2 metric tons of pressure.
Next, a wall-forming composition comprising 90% cellulose acetate having an acetyl content of 39.8%, and 10% poly(ethylene glycol) having an average molecular weight of 3350 is formed around the bilayered core. The semipermeable composition is dissolved in a mixture of acetone and water (90:10 wt:wt) to provide solid composition of the solution at 5%. The compressed bilayered cores are placed into a 61 cm coating pan and the coating solution sprayed onto the cores at a spray rate of 100 ml/min. The temperature is kept at 35°C during the coating process.

Next, one 30 mil (0.76 mm) orifice is drilled through the semipermeable wall connecting the drug composition with the exterior of the dosage form. The residual solvent is removed by drying at 45°C and 45% relative humidity in an oven for 48 hours. At the end of the drying cycle, the humidity is turned off, and the dosage forms are dried at 45°C for an additional 4 hours.

The dosage form prepared according to this example comprises a first drug layer comprising 110 mg consisting of 14.08 mg of methylphenidate, 90.26 mg of poly(ethylene oxide) of 200,000 number-average molecular weight, 5.5 mg of poly(vinylpyrrolidone) of 40,000 number-average molecular weight, 0.11 mg of magnesium stearate, and 0.055 mg of butylated hydroxy toluene. The dosage form displacement layer 2 comprises 132 mg composed of 71.032 mg of poly(ethylene oxide) of 7,000,000 number-average molecular weight, 52.8 mg of osmagent sodium chloride, 6.6 mg of poly(vinylpyrrolidone) of 40,000 number-average molecular weight, 1.32 mg of red ferric oxide, 0.132 mg of magnesium stearate, and 0.066 mg of butylated hydroxy toluene. The semipermeable wall weighed 17 mg and comprised 15.3 mg of cellulose acetate consisting of 39.8% acetyl content, and 1.7 mg of poly(ethylene glycol) of 3350 number-average molecular weight. The dosage form possessed a 30 mil (0.76 mm) orifice.

The dosage form delivered methylphenidate in an ascending release rate. The dosage from delivered 0.22 mg in the first hour, 1.45 mg in the second hour, 1.72 mg in the third hour, 1.84 mg in the fourth hour, 2.05 mg in the fifth hour, 2.21 mg in the sixth hour, 2.13 mg in the seventh hour, 1.26 mg
in the eighth hour, 0.39 mg in the ninth hour, and 0.09 mg in the tenth hour, 
with a residual of 0.72 mg in the dosage form.

EXAMPLE 2

The procedure of Example 1 is followed with the processing steps as 
previously described, except the drug in this example is a member selected 
from the group consisting of pemoline, deanol, deanol acetamidobenzoate, 
benzphetamine hydrochloride, deanol acetylglumate, clortermine, 
diethylpropion, fenfluramine, dextroamphetamine phosphate, and 
dextroamphetamine sulfate.

EXAMPLE 3

An osmotic dosage form adapted, designed and shaped as an 
oral tablet for delivering a drug with an ascending release profile is 
manufactured as follows: First, a composition is prepared by passing 
through a 40 mesh screen 393.85 g of poly(ethylene oxide) having a 
molecular weight of about 300,000. Then 63.65 g of drug selected from 
the group consisting of amphetamine sulfate, difluanine hydrochloride, 
flubanilate, mefexamide, methamphetamine, pseudoephedrine and 
pyrovalerone hydrochloride; 15.00 g of polyoxyl 40 stearate; and 25.00 g 
of hydroxypropylmethylcellulose having a number-average molecular weight 
of 11,200 are screened to 40 mesh and then added to the poly(ethylene 
oxide). The four ingredients are mixed for about 10 minutes in a conventional 
mixer. Then 50 ml of denatured, anhydrous ethanol is slowly added to the 
mixer and the mixing continued for an additional 10 minutes. The wet 
granulation is passed through a 20 mesh screen, dried at room temperature 
for 16 hours, and passed again through a 20 mesh screen. Finally, 2.5 g of 
magnesium stearate is added to the granulation and all the ingredients mixed 
for an additional 3 minutes.
Next, a second displacement composition is prepared by mixing
267.5 g of poly(ethylene oxide) having a number-average molecular weight of
7,000,000 with 175 g (35%) of osmagent sodium chloride; 25 g of Carbomer®
934, a carboxyvinyl polymer possessing a 3,000,000 number-average
molecular weight, disclosed in U.S. Patent Nos. 3,074,852, 3,634,584, and
4,248,847, commercially available from BF Goodrich Chemicals, Cleveland,
OH; and 5 g of red iron oxide. The homogenous blend is passed through a
40 mesh screen, and 25 g of hydroxypropylmethylcellulose having a number-
average molecular weight of 11,200 is added to all the ingredients. The
ingredients are blended in a conventional planetary mixer for 10 minutes.
Then, 50 ml of denatured, anhydrous ethanol is slowly added to the blending
mixture and all the ingredients mixed for an additional 5 minutes. The freshly
prepared wet granulation is passed through a 20 mesh screen, allowed to dry
at room temperature for 16 hours, and again passed through a 20 mesh
screen. The screened granulation is mixed with 2.5 g of magnesium stearate
for 3 minutes.

A laminating press is used to form the bilaminate. First, 110 mg of
the first drug composition is added to a 4.7 mm die cavity and tamped. Then,
115 mg of the second expandable composition is added to the die cavity, and
the two separate compositions pressed into a bilaminated core under 1/2 ton
of pressure.

Next, the bilaminated core is surrounded with a semipermeable wall.
The wall-forming composition comprises 95% cellulose acetate having an
acetyl content of 39.8%, and 5% polyethylene glycol having a molecular
weight of 3350. The wall forming composition is dissolved in acetone:water
(90:10 wt:wt) solvent to make a 5% solids solution. Then, 22 mg of the wall
forming composition is sprayed onto and around this bilaminate in a Hi-Coater
pan coater. Then, a 30 mil (0.76 mm) exit orifice is drilled by laser or
mechanical drill in the center of the drug laminate side of the osmotic device.
The residual solvent is removed by drying for 48 hours at 50°C and 50%
relative humidity, followed by one hour drying at 50°C.
A dosage form prepared by this example comprises a 110 mg drug layer comprising 12.73 wt% pseudoephedrine hydrochloride, 78.77 wt% poly(ethylene oxide) of 300,000 number-average molecular weight, 5 wt% hydroxypropylmethylcellulose of 11,200 number-average molecular weight, 3 wt% polyoxyl 40 stearate and 0.5 wt% magnesium stearate. The 115 mg displacement layer comprises 53.5 wt% poly(ethylene oxide) possessing a 7,000,000 number-average molecular weight, 5 wt% hydroxypropylmethylcellulose possessing 11,200 number-average molecular weight, 35 wt% sodium chloride, 0.5 wt% magnesium stearate, 5 wt% Carbopol® carboxyvinylpolymer, and 1 wt% red ferric oxide. The semipermeable wall comprises 20.9 mg of cellulose acetate of 39.8% acetyl content and 1.1 mg of poly(ethylene glycol) of 4,000 number-average molecular weight. The dosage form comprises a 30 mil orifice (0.76 mm) and exhibits the ascending release rate profile seen in accompanying Figure 1.

EXEMPLARY 4

A dosage form designed and adapted as a tablet for the oral administration of methylphenidate pharmaceutically acceptable salt in an ascending release profile is manufactured as follows: First, 163.4 g of poly(ethylene oxide) having an average molecular weight of 200,000 is passed through a 40 mesh screen and placed into the bowl of a conventional planetary mixer. Next, 25.6 g of methylphenidate hydrochloride is weighed and placed into the bowl containing the poly(ethylene oxide). Next, 10 g of hydroxypropylmethylcellulose possessing a 11,200 molecular weight is passed through a 40 mesh screen and placed into the bowl containing the poly(ethylene oxide) and methylphenidate hydrochloride. Next, 0.5 g of FD&C Blue Dye No. 1 is placed into the bowl of the mixer. The four ingredients are blended together in the planetary mixer for 10 minutes. Next, 100 ml of denatured anhydrous ethanol is gradually added to the
mixer with continued mixing for 10 minutes to change the consistency of the dry powder to that of granules. The wet granulation is then passed through a 20 mesh screen, dried at room temperature for 16 hours, and then passed through a 20 mesh screen. Next, 0.5 g of magnesium stearate, which has been passed through a 40 mesh screen, is added to the granulation, and all the ingredients are mixed for an additional 1 minute.

Next, a displacement layer is manufactured as follows: First, 107 g of poly(ethylene oxide) having an average molecular weight of 7,000,000, 80 g of sodium chloride (40%), 10 g of hydroxypropylmethylcellulose (USP grade) possessing a 11,200 molecular weight, and 2 g of red ferric oxide are passed through a 40 mesh screen and then placed into the bowl of a conventional planetary mixer. The powder mixture is then blended together until a homogenous blend is formed. Next, 50 ml of denatured anhydrous ethanol is added to the mixer with continued mixing over a period of 5 to 10 minutes, such that the consistency of the dry powder changes to granules. The wet granulation is passed through a 20 mesh screen, dried at room temperature for 16 hours, and then passed through a 20 mesh screen. Next, 1 g of magnesium stearate which has been passed through a 40 mesh screen is added to the granulation, and all the ingredients are mixed for an additional 1 minute.

Next, a bilayer press is used to compress the two layers together to form a tablet dosage form. First, 110 mg of the drug composition is added to the 4.7 mm die cavity and lightly tamped. Next, 115 mg of the displacement composition is weighed and placed into the die cavity, and the two layers are compressed together using 1/2 ton of pressure to form a bilayer pretablet.

A wall for enveloping the bilayer pretablet to yield the finished tablet is formed as follows: First, a semipermeable composition composed of 90% cellulose acetate (having an acetyl content of 39.8%) and 10% polyethylene glycol having an average molecular weight of 3350 is prepared by dissolving in a mixture of acetone and water (the solvents are mixed together in a ratio of 90:10 wt:wt), such that the solids composition of the solution is 5%. The
bilayer tablets are placed in a coater pan, and 20 mg of the semipermeable composition is sprayed on to the bilayer tablets. Next, a 30 mil (0.76 mm) orifice is drilled on the drug layer side of the bilayer tablet using an automatic tableting positioning laser drill. Next, the semipermeable coated tablets are dried for 48 hours at 50°C and 50% relative humidity to remove the residual solvents. The release rate ascending profile for a dosage form prepared according to the example is seen in accompanying Figure 2. Drawing Figure 2 depicts the release of methylphenidate hydrochloride from a semipermeable, longitudinal dosage form.

EXAMPLE 5

The procedure of the above examples is followed, with the further embodiment that a drug overcoat and an optional taste-masking coat is overcoated onto the exterior surface of the wall. The overcoat, in one manufacture, comprises 60 wt% of hydroxypropylmethylcellulose of 9,200 number-average molecular weight and 40 wt% methylphenidate hydrochloride. The hydroxypropylmethylcellulose is added to water and mixed until a uniform solution results. Then, the methylphenidate hydrochloride is added to the solution and mixed such that a clear solution results. The final solution has a solid composition of 10%.

Next, semipermeable walled dosage forms are placed in a coater and 10 mg of the drug overcoat is sprayed onto the semipermeable wall that surrounds the internal bilayer compressed tablet. Then, overcoated dosage forms are dried for 10 minutes at 40°C. For taste masking, a suspension of Opadry®, a powder blend comprised of hydroxypropylmethylcellulose, titanium dioxide, polyethylene glycol and polysorbate 80, is prepared in water to effect a solid content of 10%. The drug overcoated dosage forms are placed in a coater and 9 mg of the taste-masking solution is sprayed over the drug overcoat to produce a double-overcoated dosage form. Next, the dosage forms are dried at 40°C for 10 to 12 minutes to yield the operable dosage forms.
EXAMPLE 6

The procedures set forth in the above examples are followed, with the manufactures as described above, except in this invention, a first dosage form is provided wherein the drug layer comprises 28 mg of methylphenidate hydrochloride, and a second dosage form is provided wherein the drug layer comprises 42 mg of methylphenidate hydrochloride.

EXAMPLE 7

The procedures set forth in the above examples are followed with the manufacturing conditions set forth as previously indicated, except that in this example a dosage form is provided wherein the second displacement layer comprises 65 mg of sodium carboxymethylcellulose osmopolymer of 3,500,000 number-average molecular weight and an osmagent combination comprising 58 mg of dextrose-fructose in equal proportions; and a dosage form wherein the second displacement layer comprises 72 mg of poly(ethylene oxide)-poly(propylene oxide) copolymer of 7,900,000 number-average molecular weight and 47.8 mg of co-osmagent sodium chloride-dextrose (23.9 mg - 23.9 mg).

EXAMPLE 8

A dosage form designed and adapted to deliver a drug in an ascending release rate profile is manufactured according to this example.

First, a first layer-forming composition comprising a dose of drug is manufactured as follows: 157.8 mg of poly(ethylene oxide) having a number-average molecular weight of 200,000 is passed through a 40 mesh screen (U.S. Sieve) and placed into the bowl of a conventional planetary mixer.

Next, 31.2 g of the drug methylamphetamine hydrochloride is added to the
mixture. Then, 10 g of hydroxypropylmethylcellulose of 16,000 number-
average molecular weight is passed through a 40 mesh screen and added
to the mixer comprising the methylenedamine hydrochloride and the
poly(ethylene oxide). Then, 0.5 g of FD&C Blue Dye No. 1, for color
identification, is added to the bowl of the mixer. The ingredients are blended
in the mixer for 10 minutes to produce a homogenous composition. Next,
100 ml of denatured anhydrous ethanol is added gradually to the mixer, with
continual mixing over a period of 5 to 10 minutes to change the consistency of
the dry ingredients to wet granules. The wet granulation is passed through a
20 mesh screen, dried at room temperature for 16 hours, and then passed
through a 20 mesh screen. Then, 0.5 g of magnesium palmitate is passed
through a 40 mesh screen, added to the homogenous composition, and all
the ingredients mixed for an additional minute.

Next, a displacement layer, the second layer, is prepared as follows:
First, 53 g of poly(ethylene oxide) of 7,500,000 number-average molecular
weight, 54 g of poly(propylene oxide) of 5,000,000 number-average
molecular weight, 80 g of osmagent sodium chloride, 10 g of
hydroxypropylethylcellulose of 24,000 number-average molecular
weight, and 2 g of red ferric oxide are passed through a 40 mesh screen
and then placed into the bowl of a mixer. The ingredients are blended
together to form a homogenous blend. Next, 50 ml of denatured anhydrous
ethanol is added to the mixer, accompanied by continual mixing for
10 minutes to produce wet granules. The wet granules are passed through
a 20 mesh screen, dried at room temperature for 16 hours, and then passed
through a 20 mesh screen. Next, 1 g of stearic acid lubricant is passed
through a 40 mesh screen, added to the granulation, and all the ingredients
mixed for an additional minute.

Next, the first drug layer-forming composition and the second
displacement layer-forming composition are pressed together into contacting
layers as follows: First, 33 mg of the first composition is added to a 0.55 cm
die cavity and tamped lightly. Then, 57 mg of the displacement composition
is added to the die and tamped lightly, to provide two layers that are
compressed using 1/2 ton of pressure to form a bilayer tablet.

Next, the bilayer is surrounded with a semipermeable wall as follows:
First, a semipermeable wall forming composition is prepared comprising
95% cellulose having an acetyl content of 39.8%, and 5% polyethylene glycol
of 3350 number-average molecular weight (available from Union Carbide Co.)
by dissolving the ingredients in a mixture of acetone and water in a 90:10
(v:v) ratio to provide solid composition at 5%. The bilayer tablets are placed
in a pan coater and 15 mg of the semipermeable wall forming composition is
sprayed onto the bilayer tablet. Next, a 30 mil (0.76 mm) orifice is drilled on
the drug side to connect the first layer with the outside of the dosage form.
The dosage form tablets are dried at 50°C and 50% relative humidity to
remove the residual solvents. The dosage form comprises 5.2 mg of
methamphetamine hydrochloride to give an extended ascending release
tablet. Additional dosage forms are provided according to the invention
comprising 10 mg and 15 mg methamphetamine hydrochloride extended
ascending release tablet.

EXAMPLE 9

The above examples are followed to provide a dosage form comprising
an external coat of a pharmaceutically acceptable drug and an internal
composition comprising a pharmaceutically acceptable drug, which dosage
form when in operation in a fluid biological environment delivers the external
overcoat drug in 0 to 1 hour, and delivers the internal drug in the amounts of
15% in 0 to 2 hours, 30% in 2 to 4 hours, 33% in 4 to 6 hours, 18% in 6 to
8 hours, and 4% in 8 to 10 hours.
EXAMPLE 10

The above examples are followed to provide a dosage from comprising an external overcoat comprising 100 ng to 100 mg of drug and an internal composition comprising 10 ng to 500 mg of drug, which dosage form when in operation in the fluid environment of the gastrointestinal tract delivers the 100 ng to 100 mg external overcoat in 0 to 1 hour, and delivers the internal 10 ng to 500 mg in an increasing release of 20% in 0 to 4 hours, 30% in 4 to 8 hours, 40% in 8 to 12 hours and 10% in 12 to 16 hours, to substantially overcome tolerance to delivered drug.

EXAMPLE 11

An osmotic dosage form designed and shaped to deliver methylphenidate hydrochloride to a patient in need of methylphenidate therapy in an ascending release profile is manufactured as follows:

Composition of drug layer 1: The following procedure is used to manufacture 8,000 g of layer 1 composition:

A. Preparation of binder solution.

260 g of hydroxypropylmethylcellulose having average molecular weight of 11,200 is added to a mixing vessel containing 3250 g of water. This mixture is stirred until the hydroxypropylmethylcellulose dissolves in water and a clear solution is formed. This solution is referred to as the binder solution.

B. Preparation of methylphenidate hydrochloride granules.

4380 g of polyethylene oxide having an average molecular weight of 200,000 is passed through a 40 mesh screen. Then, 2190 g of the screened poly(ethylene oxide) is placed into the bowl of a fluid bed granulator. Next, 2032 g of sorbitol is added to the powder bed, followed by 1024 g of methylphenidate hydrochloride into the bowl over the poly(ethylene oxide). Next, 140 g of hydroxypropylmethylcellulose is added
to the bowl. The remaining 2190 g of poly(ethylene oxide) is then added to the bowl. The addition of dry ingredients into the bowl is performed so that the methylphenidate hydrochloride is located in between the two layers of poly(ethylene oxide). The bowl is attached to the main body of the granulator and the granulation process is initiated. Initially, the powder bed inside the bowl is fluidized for 2 minutes to obtain uniform mixing of the powders. Next, the binder solution is sprayed onto the powder bed through nozzles such that the solution is sprayed at a rate of 60 g/min. During the spraying process, the process air flow is maintained at 500 cfm and the product temperature is maintained at 22°C. During the spraying operation, the solution is sprayed for 30 seconds followed by a shaking time of 10 seconds, during which time the powders adhering to the filterbags may be dislodged into the granulating chamber. At the end of the spraying operation, the granules are dried in the granulating chamber for an additional 5 to 10 minutes to obtain dry granulation. The methylphenidate hydrochloride granules are then passed through a fluid air mill with a 7 mesh screen for size reduction. The size-reduced granules are then placed into a suitable blender. 160 g of magnesium stearate (screened through a 40 mesh screen) and 4 g of powdered butylated hydroxy toluene (screened through a 60 mesh screen) are added to the granules and mixed together.

Composition of layer 2: The following procedure is used to manufacture 8,000 g of displacement layer 2 composition:

A. Preparation of binder solution.

260 g of hydroxypropylmethylcellulose having an average molecular weight of 11,200 is added to a mixing vessel containing 3250 g of water. This mixture is stirred until the hydroxypropylmethylcellulose dissolves in water and a clear solution is formed. This solution is referred to as the binder solution.

B. Preparation of osmotic layer granules.

4308 g of poly(ethylene oxide) having an average molecular weight of 7,000,000 is placed into the bowl of a fluid bed granulator. Next, 140 g of
hydroxypropylmethylcellulose having an average molecular weight of 11,200
is added to the bowl. Then, 3,200 g of sodium chloride and 80 g of red ferric
oxide, which have been screened using a 21 mesh screen, are then placed
into the bowl. The bowl is attached to the main body of the granulator and
the granulation process is then initiated. Initially, the powder bed inside the
bowl is fluidized for 3 minutes to obtain uniform mixing of the powders. Next,
the binder solution is sprayed onto the powder bed through nozzles, such that
the solution is sprayed at a rate of 80 g/min. During the spraying process, the
process air flow is maintained at 400 cfm, and the product temperature is
maintained at 22°C. During the spraying operation, the solution is sprayed for
30 seconds followed by a shaking time of 10 seconds, during which time the
powders adhering to the filterbags may be dislodged into the granulating
chamber. At the end of the spraying operation, the granules are dried in the
granulating chamber for an additional 10 to 15 minutes to obtain dry
granulation. The process parameters may be adjusted to obtain a quality
product. The granules then are passed through a fluid air mill with a 7 mesh
screen for size reduction. The size-reduced granules are then placed into a
suitable blender. Next, 8 g of magnesium stearate (screened through a
40 mesh screen) and 4 g of powdered butylated hydroxy toluene (screened
through a 60 mesh screen) are added to the granules and mixed together.

C. Compression of the layers.
The methylphenidate granules-forming layer and the osmotic granules-
forming layer are compressed together using an automated tablet
compression machine capable of compressing the two layers together
longitudinally. First, 110 mg of methylphenidate granules (layer 1) is added
into the die cavity of a 3/16" diameter modified ball tooling, tamped, and then
132 mg of the osmotic layer granulation (layer 2) is placed into the die and
compressed together using 0.2 metric tons of pressure.

D. Application of semipermeable membrane wall.
The semipermeable membrane wall is composed of 47.5% cellulose
acetate (having an acetyl content of 39.8), 47.5% cellulose acetate (having an
acetyl content of 32.0), and 5% polyethylene glycol having an average
molecular weight of 3350. The semipermeable membrane-forming
composition is dissolved in a mixture of methylene chloride and methanol
(the solvents are mixed together in a ratio of 80:20 wt:wt), such that the solids
composition of the solution is 4%. The compressed systems are placed into a
61 cm coating pan and the coating solution is sprayed onto the tablets such
that the solution is sprayed at a rate of 100 ml/min/gun. The product
temperature is maintained at 25°C; the coating process is stopped when the
semipermeable membrane composition has been sprayed onto the
compressed systems.

Next, one 30 mil (0.76) orifice is drilled, using a mechanical drill bit or a
laser, on the drug layer side of the coated systems. The residual solvents
remaining after the coating are removed by drying the systems at 45°C and
45% relative humidity in an oven for 48 hours. At the end of this drying cycle,
the humidity is turned off, and the systems are dried at 45°C for an additional
4 hours to complete the drying process.

A methylphenidate dosage form assembled as described contains
110 mg of drug containing layer 1, which is composed of 12.8%
methylphenidate hydrochloride, 54.75% poly(ethylene oxide) of average
molecular weight 200,000, 25.4% sorbitol, 5% hydroxypropylmethylcellulose
of average molecular weight 11,200, 2% magnesium stearate and 0.05%
butylated hydroxy toluene. The dosage form also contains 132 mg of layer 2,
composed of 53.85% poly(ethylene oxide) of average molecular weight
7,000,000, 40% sodium chloride, 5% hydroxypropylmethylcellulose of
average molecular weight 11,200, 1% red ferric oxide, 0.1% magnesium
stearate and 0.05% butylated hydroxy toluene. The 42 mg semipermeable
laminate is composed of 47.5% cellulose acetate of acetyl content 39.8% and
47.5% cellulose acetate of acetyl content 32.0%, and 5% polyethylene glycol
having an average molecular weight of 3350 is applied to the compressed
bilayer system. A 30 mil (0.76 mm) orifice is drilled on the drug layer side
as the exit orifice. The final system is capable of delivering 14 mg of
methylphenidate hydrochloride with an ascending release rate profile
over time.

The dosage form delivered methylphenidate hydrochloride in an
ascending rate. The dosage form delivered 0.13 mg in the first hour, 1.16 mg
in the second hour, 1.53 mg in the third hour, 1.61 mg in the fourth hour,
1.75 mg in the fifth hour, 1.79 mg in the sixth hour, 2.13 mg in the seventh
hour, 2.18 mg in the eighth hour, 1.07 mg in the ninth hour, and 0.43 mg in
the tenth hour, 0.17 mg in the eleventh hour, and 0.13 mg in the twelfth hour.

**EXAMPLE 12**

An osmotic dosage form designed, shaped and adapted for delivering
methylphenidate pharmaceutically acceptable salt to a patient in need of
methylphenidate therapy in an ascending release rate profile is manufactured
as follows: First, the procedure used to manufacture the drug layer
granulation in Example 11 is followed in this example. The composition of
the drug layer can comprise from 0% to 30% sorbitol. Next, the following
procedure is used to manufacture the displacement layer:

**A. Preparation of binder solution.**

400 g of hydroxypropylmethylcellulose having an average molecular
weight of 11,200 is added to a mixing vessel containing 5000 g of water.
This mixture is stirred until the hydroxypropylmethylcellulose dissolves in
water and a clear solution is formed. This solution is referred to as the binder
solution.

**B. Preparation of osmotic layer granules.**

First, 3912 g of hydroxyethylcellulose having an average molecular
weight of 1,300,000 is placed into the bowl of a fluid bed granulator. Next,
400 g of hydroxypropylmethylcellulose having an average molecular weight of
11,200 is added to the bowl. Then, 3,200 g of sodium chloride and 80 g of
black ferric oxide, which have been milled using a 21 mesh screen, is then
placed into the bowl. The bowl is attached to the main body of the granulator
and the granulation process is then initiated. Initially, the powder bed inside
the bowl is fluidized for 3 minutes to obtain uniform mixing of the powders.
Next, the binder solution is sprayed at a rate of 80 g/min. During the spraying
process, the process air flow is maintained at 400 cfm and the product
temperature is maintained at 22°C. During the spraying operation, the
solution is sprayed for 30 seconds followed by a shaking time of 10 seconds,
during which time the powders adhering to the filterbags may be dislodged
into the granulating chamber. At the end of the spraying operation,
the granules are dried in the granulating chamber for a additional 10 to
15 minutes to obtain dry granulation. The process parameters may be
adjusted to obtain a quality product. The granules are then passed through
a fluid air mill with a 7 mesh screen for size reduction. The size-reduced
granules are then placed into a blender. Then, 8 g of magnesium stearate
(screened through a 40 mesh screen) and 4 g of powdered butylated hydroxy
toluene (screened through a 60 mesh screen) is added to the granules and
mixed together.

C. Compression of the layers.

The methylphenidate granules-forming layer and the osmotic granules-
forming layer are compressed together using an automated tablet
compression machine capable of compressing the two layers together
longitudinally. First, 110 mg of methylphenidate granules (layer 1) is added
into the die cavity of a 3/16" diameter tooling, tamped, and then 132 mg of the
osmotic layer granulation (layer 2) is placed into the die and compressed
together using 0.2 metric tons of pressure.

D. Application of semipermeable membrane wall.

The semipermeable membrane wall forming composition is composed
of 47.5% cellulose acetate 398 (having an acetyl content of 39.8), 47.5%
cellulose acetate 320 (having an acetyl content of 32.0) and 5% polyethylene
glycol having an average molecular weight of 3350. The semipermeable
membrane composition is dissolved in a mixture of methylene chloride and
methanol (the solvents are mixed together in a ratio of 80:20, wt:wt), such that
the solids composition of the solution is 4%. The compressed systems are
placed into a 24" coating pan and the coating solution is sprayed onto the
tablets such that the solution is sprayed at a rate of 100 ml/min/gun.
The product temperature is maintained at 35°C. The coating process is
stopped when the desired amount of semipermeable membrane composition
has been sprayed onto the compressed systems.

Next, one 30 mil (0.76 mm) orifice is drilled using a laser, on the drug
layer side of the coated systems. The residual solvents remaining after the
coating are removed by drying the systems at 45°C and 45% relative humidity
in an oven for 48 hours. At the end of this drying cycle, the humidity is turned
off and the systems are dried at 45°C for an additional 4 hours to complete
the drying process.

A methylphenidate dosage form assembled as described
contains 110 mg of drug containing layer 1, which is composed of 12.8%
methylphenidate hydrochloride, 50.2% to 80.2% poly(ethylene oxide)
of average molecular weight 200,000, 0 to 30% sorbitol,
5% hydroxypropylmethylcellulose of average molecular weight 11,200,
2% magnesium stearate, and 0.05% butylated hydroxy toluene.
The dosage form also contains 132 mg of layer 2, composed of 48.9%
hydroxyethylcellulose of average molecular weight 1,300,000, 40% sodium
chloride, 5% hydroxypropylmethylcellulose of average molecular weight
11,200, 1% red ferric oxide, 0.1% magnesium stearate and 0.05% butylated
hydroxy toluene. 42 mg of a semipermeable laminate composed of 47.5%
cellulose acetate of acetyl content 39.8%, 47.5% cellulose acetate of acetyl
content 32.0%, and 5% polyethylene glycol having an average molecular
weight of 3350 is applied to the compressed bilayer system, and a 30 mil
(0.76 mm) orifice is drilled on the drug layer side as the exit orifice. The final
system is capable of delivering 14 mg of methylphenidate hydrochloride with
an ascending release rate profile over a prolonged period of time.
EXAMPLE 13

The manufacturing procedures described in the above examples are followed, except that in this example a dosage form is provided wherein a drug overcoat and an optional taste-masking coat is overcoated onto the semipermeable walled dosage form. In this example, the drug layer is composed of 14 mg methylphenidate hydrochloride, 27.5 mg sorbitol, 5.5 mg polyvinylpyrrolidone, 61 mg of poly(ethylene oxide) of average molecular weight 2,000,000, 2.2 mg of magnesium stearate and 0.055 mg of butylated hydroxy toluene. The second displacement layer is composed of 72 mg of poly(ethylene oxide) of average molecular weight 7,000,000, 53 mg of sodium chloride, 6.6 mg of polyvinylpyrrolidone, 1.3 mg of ferric oxide, 0.132 mg of magnesium stearate, and 0.066 mg of butylated hydroxy toluene. The semipermeable wall is composed of 20 mg of cellulose acetate of average acetyl content 39.8%, 20 mg of cellulose acetate of average acetyl content 32% and 2 mg of poly(ethylene oxide) of average molecular weight 4000.

The drug-containing overcoat is composed of 60% hydroxypropylmethylcellulose and 40% methylphenidate hydrochloride. The hydroxypropylmethylcellulose is added to water and mixed until a uniform solution results. Then, the methylphenidate hydrochloride is added to this solution and mixed such that a clear solution results. The final solution has a solids composition of 10%. The semipermeable walled dosage forms are placed in a coater and 10 mg of the drug overcoat is sprayed onto the semipermeable wall that surrounds the internal bilayer compressed tablet.

Next, the tablets are dried in the coating pan at 40°C for 10-15 minutes. For the taste masking coat, a suspension of Opadry® is prepared in water such that the solids content is 10%. Opadry® is a powder blend commercially available from Colorcon Inc., and is composed of hydroxypropylmethylcellulose, titanium dioxide, polyethylene glycol and polysorbate 80. The systems coated with the drug containing overcoat are
placed into the coater, and the 9 mg of taste-masking coating solution is sprayed onto the systems. Next, the systems are dried in the coating pan at 40°C for 10-15 minutes to yield the operable dosage forms.

The accompanying Figure 3 represents the functionality of the dosage form of the example. The dosage form releases 4 mg of drug in the first half hour from the drug overcoat, followed by 0.41 mg in the next half hour, 1.05 mg in the second hour, 1.49 mg in the third hour, 1.57 mg in the fourth hour, 1.71 mg in the fifth hour, 1.75 mg in the sixth hour, 2.09 mg in the seventh hour, 2.14 mg in the eighth hour, 1.32 mg in the ninth hour and 0.48 mg in the tenth hour.

EXAMPLE 14

The dosage form is manufactured as described in Example 13, wherein in the second displacement layer the poly(ethylene oxide) is replaced with 72 mg of hydroxyethylcellulose of 1,300,000 molecular weight.

EXAMPLE 15

Dosage forms are provided according to the above examples wherein:
(a) the dosage form comprises an overcoat of 8 mg of methylphenidate and an internal composition comprising 28 mg of methylphenidate; and (b) the dosage form comprises an overcoat of 12 mg of methylphenidate, and an internal composition comprising 42 mg of methylphenidate.

EXAMPLES 16 TO 19

Dosage forms are provided by following the above disclosure and examples to provide dosage forms that deliver a dose of drug, for example, a central nervous system drug, in an ascending profile in the following therapeutic ranges: (a) a dosage form that delivers in the first hour 0 to
0.308 mg of drug, in the second hour 0.250 mg to 2 mg of drug, in the third
hour 1 mg to 2.4 mg of drug, in the fourth hour 1.1 mg to 2.6 mg of drug, in
the fifth hour 1.23 mg to 2.9 mg of drug, in the sixth hour 1.33 mg to 3.1 mg
of drug, in the seventh hour 1.28 to 2.98 mg of drug, and in the eighth hour
0.76 mg to 1.76 mg of drug; (b) a dosage form exhibiting an ascending dose
profile in the first hour 0 mg to 3.00 mg, in the second hour 2.75 mg to 10 mg,
in the third hour 5 mg to 12 mg, in the fourth hour 5.5 mg to 13 mg, in the fifth
hour 6.15 mg to 14.5 mg, in the sixth hour 6.65 to 15.5 mg, in the seventh
hour 6.4 mg to 14.9 mg, and in the eighth hour 3.8 to 8.8 mg; (c) a dosage
form comprising a drug ascending release rate program of 0 mg to 0.400 mg
in the first hour, 0.376 mg to 1.81 mg in the second hour, 1.29 mg to 2.15 mg
in the third hour, 1.38 mg to 2.3 mg in the fourth hour, 1.54 mg to 2.57 mg in
the fifth hour, 1.66 mg to 2.76 mg in the sixth hour, 1.59 to 2.66 mg in the
seventh hour, and 0.93 to 1.58 mg in the eighth hour; and (d) a dosage form
that delivers an orally administrable drug in an ascending dose of 0 mg to
3.00 mg in the first hour, 2.45 mg to 9.05 mg in the second hour, 6.45 mg to
10.75 mg in the third hour, 6.9 mg to 11.5 mg in the fourth hour, 7.7 mg to
12.9 mg in the fifth hour, 8.3 mg to 13.8 mg in the sixth hour, 7.95 mg to
133 mg in the seventh hour, and 4.65 mg to 7.9 mg in the eighth hour.

EXAMPLES 20 TO 21

The procedures set forth in the above examples are followed with the
manufacture as described above, except in this invention, a first dosage form
is provided wherein the drug layer comprises 28 mg of methylphenidate
hydrochloride and a second dosage form is provided where the drug layer
comprises 42 mg of methylphenidate hydrochloride.
DISCLOSURE OF METHOD OF USING THE INVENTION

The invention pertains further to methods for delivering an ascending dose over time to a warm-blooded animal in need of therapy. The invention provides: (a) a method for delivering a dose of drug in an increasing rate to a patient, wherein the method comprises administering orally to the patient a drug in an increasing rate per hour over time, to provide the dose of drug to the patient; (b) a method for delivering a dose of drug in an increasing dose of drug to a patient, wherein the method comprises delivering orally to the patient an orally administrable drug, in an increasing milligram dose per hour over twenty-four hours, to deliver the dose of drug; (c) a method for delivering a drug to a patient from a dosage form over time, wherein the method comprises admitting orally into the patient a dosage form comprising 240 nanograms to 700 milligrams of drug that is delivered in an increasing dose over time; and (d) a method comprising the steps of: (A) admitting into a patient a dosage form comprising: (1) a wall that surrounds a compartment, the wall comprising a semipermeable composition permeable to the passage of fluid, including aqueous-biological fluid of the gastrointestinal tract, and impermeable to the passage of drug; (2) a bilayer in the compartment comprising a first layer comprising a dose of drug, a second layer comprising an osmopolymer, or an osmopolymer and an osmagent, and for imbibing and absorbing fluid for pushing the first layer from the dosage form and thereby providing an increased dose per unit time over time; and (3) at least one exit in the wall communicating with the first layer; (B) imbibing fluid through the semipermeable wall at a rate determined by the permeability of the semipermeable wall and the osmotic gradient across the semipermeable wall causing the second layer to expand and swell; and (C) deliver the drug from the first layer through the exit passageway to provide an ascending, increasing dose of drug to the patient.
In summary, it will be appreciated the present invention contributes to the art an unexpected dosage form that possesses the practical utility for administering a sustained and increasing dose of drug at a dosage-metered release rate over time. While the invention has been described and pointed out in detail with reference to operative embodiments thereof, it will be understood to those skilled in the art that various changes, modifications, substitutions and omissions can be made without departing from the spirit of the invention. It is intended, therefore, that the invention embraces those equivalents within the scope of the claims.
We claim:

1. An osmotic tablet for administering a dose of drug to a patient, wherein the osmotic tablet comprises:
   (a) a drug composition comprising 10 ng to 700 mg of drug; and
   (b) an expandable composition comprising 100 ng to 400 mg of a hydrophilic-expandable polymer; and wherein the drug composition and the expandable composition are in contacting arrangement, and the osmotic tablet administers the drug in an ascending-release rate to the patient.

2. The osmotic tablet for administering a dose of drug to a patient, according to claim 1, wherein the drug is a member selected from the group consisting of an opioid, barbiturate, hypnotic, central nervous system acting drug, psychostimulant, psychodepressant, cannabinoid and catecholamine.

3. The osmotic tablet for administering a dose of drug to a patient according to claim 1, wherein the drug is a member selected from the group consisting of amphetamine, dextroamphetamine, methamphetamine, methylphenidate, racemic methylphenidate, alklyphenidate, ethylphenidate, throleethylphenidate, phenylisopropylamine, and pemoline.

4. The osmotic tablet for administering a dose of drug to a patient according to claim 1, wherein the drug is a pharmaceutically acceptable salt.

5. The osmotic tablet for administering a dose of drug to a patient according to claim 1, wherein the osmotic tablet imbibes fluid from the patient and administers the dose of drug.

6. An osmotic tablet for administering a dose of drug to a patient, wherein the osmotic tablet comprises:
   (a) a drug layer comprising 10 ng to 700 mg of drug; and,
   (b) a osmotic layer comprising 80% to 95% of a composition comprising an osmopolymer and an osmagent; and wherein the drug layer and the osmotic layer comprise a bilayer that administers the drug in an ascending-release rate to the patient.
7. The osmotic tablet for administering a dose of drug to a patient according to claim 6, wherein the drug is a member selected from the group consisting of an opioid, barbiturate, hypnotic, central nervous system acting drug, psychostimulant, psychodepressant, cannabinoid, and catecholamine.

8. The osmotic tablet for administering a dose of drug to a patient according to claim 6, wherein the drug comprises a member selected from the group consisting of amphetamine, dextroamphetamine, methamphetamine, alkylphenidate, methylphenidate, racemic methylphenidate, ethylphenidate, threomethylphenidate, phenylisopropylamine, and pemoline.

9. The osmotic tablet for administering a drug to a patient according to claim 6, wherein the drug is a pharmaceutically acceptable salt selected from the group consisting of hydrochloride, hydrobromide, fumarate, phosphate, sulfate, lactate, malate, acetate, tartrate, citrate, pamoate, maleate, ascorbate, gluconate, aspartate and salicylate.

10. The osmotic tablet for administering a drug to a patient according to claim 6, wherein the osmotic tablet an oral administration to the patient imbibes fluid and administers the drug.

11. The osmotic tablet for administering a drug to a patient according to claim 6, wherein a composition comprising a polymer envelops the osmotic tablet.

12. The osmotic tablet for administering a drug to a patient according to claim 6, wherein the osmotic tablet is longer than wide.

13. The osmotic tablet for administering a drug to a patient according to claim 6, wherein the osmotic tablet is longer than thick.

14. A dosage form comprising:
   (a) a first layer comprising 10 ng to 700 mg of drug;
   (b) a second layer comprising 80% to 95% of a hydrophilic-expandable polymer;
   (c) a wall comprising a semipermeable composition that surrounds the first and second layer;
(d) an exit in the wall communicating with the first layer for delivering the drug; and wherein the dosage form when in operation administers the drug in an ascending rate over time.

15. The dosage form according to claim 14, wherein the first layer comprises a drug selected from the group consisting of an opioid, barbiturate, hypnotic, central nervous system acting drug, psychostimulant, psychodepressant, cannabinoid, and catecholamine.

16. The dosage form according to claim 14, wherein the first layer comprises a drug selected from the group consisting of amphetamine, dextroamphetamine, methamphetamine, methylphenidate, racemic methylphenidate, alkylphenidate, ethylphenidate, threonethylphenidate, phenylisopropylamine, and pemoline.

17. The dosage form according to claim 14, wherein the dosage form comprises a length greater than its width and is designed for administering the drug in an ascending-increasing dose over a sustained time.

18. The dosage form according to claim 14, wherein the dosage form comprises a length in excess of its width and the second layer comprises 80% to 95% hydrophilic-expandable polymer that provides for an ascending-increasing dose of drug over a sustained period.

19. The dosage form according to claim 1, wherein the first layer comprises a poly(alkylene oxide) of 25,000 to 1,000,000 number-average molecular weight.

20. The dosage form according to claim 14, wherein the first layer comprises a carboxyvinylpolymer of 7,500 to 1,000,000 number-average molecular weight.

21. The dosage form according to claim 14, wherein the first layer comprises a carboxyalkylcellulose of 10,000 to 700,000 molecular weight.

22. The dosage form according to claim 14, wherein the second layer comprises a poly(alkylene oxide) of 2,500,000 to 10,000,000 number-average molecular weight.
23. The dosage form according to claim 14, wherein the second layer comprises a carboxyalkylcellulose of 1,750,000 to 10,000,000 number-average molecular weight.

24. The dosage form according to claim 14, wherein the first and second layers comprise a hydroxypropylalkylcellulose.

25. The dosage form according to claim 14, wherein the first and second layers comprise a hydroxyalkylcellulose.

26. A dosage form comprising:
   (a) a first layer comprising 10 ng to 700 mg of drug;
   (b) a second layer comprising a composition comprising 80% to 95% of a osmopolymer and an osmagent;
   (c) a wall comprising a semipermeable composition that surrounds the first and second layers;
   (d) an exit in the wall communicating with the first layer for delivering the drug; and wherein the dosage from when in operation administers the drug in an increasing sustained dose over time.

27. The dosage form according to claim 24, wherein an overcoat comprising a drug is on the exterior surface of the wall.

28. The dosage form according to claim 24, wherein the first layer comprises a drug selected from the group consisting of amphetamine, dextroamphetamine, methamphetamine, methylphenidate, racemic methylphenidate, alkylphenidate, ethylphenidate, threomethylphenidate, phenylisopropylamine, and pemoline.

29. The dosage form according to claim 24, wherein the dosage form comprises a length in excess of its width.

30. The dosage form according to claim 24, wherein the dosage form comprises a length in excess of its thickness.

31. The dosage form according to claim 24, wherein the second layer composition comprising the osmopolymer and the osmagent combine with the dosage form design to deliver the drug in an increasing sustained dose over time.
32. The dosage form according to claim 24, wherein the first and second layers comprise a poly(alkylene oxide) and the poly(alkylene oxide) in the second layer has a higher number-average molecular weight.

33. The dosage form according to claim 24, wherein the first and second layers comprise a carboxyalkylcellulose and the carboxyalkylcellulose in the second layer comprises a higher molecular weight.

34. The dosage form according to claim 24, wherein the first and second layers comprise a hydroxypropylalkylcellulose.

35. The dosage form according to claim 24, wherein the first and second layers comprise a hydroxyalkylcellulose in an increasing dose over time, wherein the method comprises admitting orally into the patient a dosage from comprising 240 nanograms to 700 milligrams of drug that delivers the drug in an increasing dose per hour over time to deliver the dose of drug to the patient.
**INTERNATIONAL SEARCH REPORT**

**A. CLASSIFICATION OF SUBJECT MATTER**

IPC 6 A61K9/22

According to International Patent Classification (IPC) or to both national classification and IPC.

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61K

Documentation searched other than minimum: documentation to the extent that such documents are included in the fields searched.

Electronic database consulted during the international search (name of database and, where practical, search terms used).

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

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Further documents are listed in the continuation of box C.

Special categories of cited documents:

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Date of the actual completion of the international search: 23 April 1998

Date of mailing of the international search report: 06/05/1998

Name and mailing address of the ISA:
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Authorized officer: Boulois, D

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