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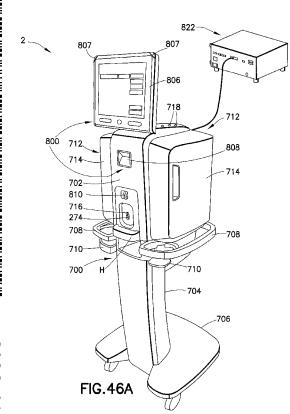
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[Continued on next page]

(54) Title: CONTINUOUS MULTI-FLUID DELIVERY SYSTEM AND METHOD



(57) Abstract: A fluid pump device is operable by a drive and actuating system. The fluid pump device includes a pump manifold, a plurality of pump cylinders, a plunger reciprocally operable in each of the pump cylinders, and at least one inlet selector valve. The pump cylinders may extend proximally from the pump manifold and are in selective fluid communication with the pump manifold via, for example, respective inlet and outlet check valves. The plungers are reciprocally operable within the pump cylinders and are independently and reciprocally operable by respective piston linear actuators provided in the drive and actuating system. The inlet selector valve is used to establish selective fluid communication between one or more fluid source containers and the pump manifold to control fluid flow into the pump manifold. The inlet selector valve may be located laterally outboard of the pump cylinders and extend generally parallel to the pump cylinders.



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CONTINUOUS MULTI-FLUID DELIVERY SYSTEM AND METHOD

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This application claims the benefit of United States Provisional Application No. 61/537,371, filed September 21, 2011 and entitled "Continuous Multi-Fluid Delivery System and Method", and which is incorporated herein in its entirety.

BACKGROUND OF THE INVENTION

Field of the Invention

[0002] The invention described herein is directed to a fluid delivery system comprising a fluid pump device and an associated drive and actuating system for continuous multi-fluid delivery applications in medical diagnostic and therapeutic procedures wherein one or more fluids are infused/injected into a patient.

Description of Related Art

[0003] In the medical field, fluid delivery devices used to provide fluids to patients are generally well-known and exist in many different forms. A system commonly used for this purpose is a gravity-feed system wherein a fluid containing bag is supported above the level of the patient's body and wherein the flow rate to the patient is controlled by the gross pressure of a clamp upon the flexible tube extending between the bag and the patient. It will be readily understood that the flow rate of fluid through the tube is a function of the amount of constriction of the tube. Manually operated devices are known in the medical field for delivery of fluid under pressure to a patient. Examples of such manually-operated pumping devices are known from United States Patent Nos. 3,464,359 to King et al.; 2,062,285 to Bergman; and 1,748,810 to Wandel, as examples.

[0004] Syringe-based infusion pumps and peristaltic pumps have also been used in the medical field for delivering fluids to patients under pressure and provide more precise control over the flow rate and volumetric delivery of fluids to patients. An example of a syringe pump adapted to deliver fluid to a patient is described in United States Patent No. 5,529,463 to Layer et al., which discloses a multi-syringe pump for this purpose. A peristaltic pump system suitable for delivering a constant flow of fluid under pressure to a patient is described in United States Patent Nos. 6,558,125 and 6,488,660, both to Futterknecht.

[0005] There are a number of medical procedures which require the delivery of fluids to a patient in a precisely controlled manner. One such application involves the delivery of contrast media fluid to a patient during a diagnostic computed tomography (CT) scan to

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provide enhanced x-ray images. Traditionally, such contrast media fluid has been delivered to the patient using a syringe-based injection system. Such injection systems require the contrast media fluid to be transferred from its original container to a disposable syringe. The injection system then pressurizes the fluid within the syringe to deliver the fluid to the patient at a controlled flow rate, precisely when needed. Some syringe-based injection systems are capable of accommodating two separate syringes to facilitate sequential or simultaneous delivery of two different types of fluid.

[0006] One limitation of a syringe-based fluid injection system is the need to refill and replace the disposable syringes prior to each patient procedure. United States Patent No. 5,806,519 to Evans, III et al. describes a fluid delivery system which could be used to deliver fluid to multiple patients in succession without the need to refill and replace syringes for each patient. Another fluid delivery system that purports to overcome this limitation is disclosed in United States Patent Nos. 6,558,125 and 6,488,660 (Futterknecht). These latter patents disclose a fluid delivery system that utilizes a peristaltic pump to deliver fluid directly from contrast media bottles to the patient. While this system eliminates the need to replace disposable syringes after each patient, the use of a roller-type peristaltic pump inherently limits the pressure capability of the system to approximately 200 psi. Unfortunately, many CT procedures and virtually all angiographic procedures require fluid to be delivered at higher pressures.

[0007] In order to provide more precise control of flow rates and volumetric delivery of fluids to patients, positive displacement pump platforms have been developed in the medical field. These devices eliminate the use of syringes and provide increased pressure ranges over peristaltic pumps. One such positive displacement pump device is disclosed in United States Patent Nos. 5,196,197 and 6,197,000 to Reilly et al., which describe a system for the continuous delivery of contrast media fluid to a patient that uses a cam-driven multi-piston pump. Such a pump is capable of delivering fluids at relatively high pressures in a controlled manner. Another example of a positive displacement pump platform intended for use in delivering fluid to a patient undergoing a medical procedure is disclosed in International Publication No. WO 2006/056828, which discloses a volumetric pump with reciprocating and rotating pistons that are adapted to deliver a controlled and continuous flow rate of fluid during a medical procedure. Japanese Publication Nos. JP 61-42199 and JP 61-4220, both assigned to Nemoto Kiyourindou KK, disclose another multi-piston cylinder pump which enables the controlled and continuous delivery of fluids during a medical procedure.

[8000] There are several disadvantages present in positive displacement pump platforms known in the medical field for fluid delivery to a patient. One disadvantage is that these pump platforms are, typically, limited to pumping a single fluid type. Many medical procedures, such as CT procedures, often involve the use of a combination of contrast media fluid and saline delivered precisely to the region of interest within a patient's body. For example, after an initial injection of contrast media fluid is performed, a bolus of saline fluid may be administered to move the contrast fluid into the region of interest. In order to have the capability of delivering two or more different types of fluids, an external selection valve (such as a stopcock) must be added upstream of the pump inlet to allow the fluid delivery system to select from one of the two available fluid sources or possibly both if a mixing device is also provided. If two interconnected pumps are present in the fluid delivery system, the system may be capable of delivering a controlled mixture of two fluids. However, each of the two pumps must be independently controlled to provide the required flow rate of its respective fluid type. Downstream mixing devices may also be used in such a two-pump system.

SUMMARY OF THE INVENTION

[0009] This disclosure presents exemplary embodiments of a fluid pump device for association with a drive and actuating system, exemplary embodiments of the drive and actuating system, and exemplary embodiments of a fluid delivery system comprising the drive and actuating system and fluid pump device, as well as methods of assembling the fluid pump device and methods of operating one or more embodiments of the fluid pump device, drive and actuating system, and fluid delivery system. In one embodiment, a fluid pump device comprises a plurality of pump cylinders, a plunger reciprocally operable within each of the pump cylinders, and an inlet selector valve to establish selective fluid communication between at least one fluid source and the pump cylinders. The inlet selector valve may be located laterally outboard of the pump cylinders.

[0010] The inlet selector valve may be oriented generally parallel to the pump cylinders. The fluid pump device may further comprise a pump manifold controlling fluid communication to the pump cylinders, and the inlet selector valve controls fluid communication with the at least one fluid source to control fluid flow into the pump manifold. The pump manifold comprises an inlet manifold channel and an outlet manifold channel, and further comprises an outlet selector valve in fluid communication with the outlet manifold channel to control fluid flow from the pump manifold. The outlet selector valve

comprises an outlet selector valve cylinder having a valve stem disposed therein, and wherein the outlet selector valve comprises a patient outlet port and a waste outlet port. The outlet selector valve stem defines a flow passage to establish selective fluid communication with the patient outlet port or the waste outlet port. The outlet selector valve stem may define a tapered end. The pump manifold may comprise an inlet manifold channel and an outlet manifold channel, and the pump cylinders may each comprise at least one inlet opening for fluid communication with the inlet manifold channel and at least one outlet opening for fluid communication with the outlet manifold channel. The pump cylinders may be in selective fluid communication with the inlet manifold channel and the outlet manifold channel via respective inlet check valves and outlet check valves. The at least one outlet opening may be positioned at a high point in each of the pump cylinders for air bubble egress.

[0011] The inlet selector valve may comprise an inlet selector valve cylinder having a valve stem disposed therein, the valve stem defining an axial passage and a plurality of radial inlet ports connected to the axial passage. The radial inlet ports may be disposed at different angular orientations around the valve stem. The radial inlet ports may alternatively be disposed at different angular orientations around the valve stem and at different axial locations along the valve stem. A saline manifold may be in selective fluid communication with the pump cylinders via the inlet selector valve to establish selective fluid communication between a saline fluid source and the pump cylinders. The saline manifold may extend across the plurality of pump cylinders.

[0012] In another embodiment, the fluid pump device may comprise a plurality of pump cylinders, a plunger reciprocally operable within each of the pump cylinders, and an inlet selector valve to establish selective fluid communication between at least one fluid source and the pump cylinders. The inlet selector valve may be located laterally outboard of the pump cylinders, and identifying indicia may be provided on the fluid pump device and encoded with identifying information for the fluid pump device.

[0013] The inlet selector valve may comprise an inlet selector valve cylinder having a valve stem disposed therein, the valve stem defining an axial passage and plurality of radial inlet ports connected to the axial passage, and the identifying information comprising at least an initial angular orientation of the valve stem in the inlet selector valve cylinder or a representation thereof. The radial inlet ports may be disposed at different angular orientations around the valve stem. Alternatively, the radial inlet ports may be disposed at different angular orientations around the valve stem and at different axial locations along the valve

stem. The inlet selector valve cylinder may be oriented generally parallel to the pump cylinders.

[0014] The identifying indicia may be an optically encoded transparent member. The identifying indicia may be disposed on one of the pump cylinders. The inlet selector valve may comprise an inlet selector valve cylinder having a valve stem disposed therein, and the identifying information may comprise at least an initial angular orientation of the valve stem in the inlet selector valve cylinder or a representation thereof. The valve stem may comprise a plurality of radial inlet ports disposed at different angular orientations around the valve stem. Alternatively, the valve stem may comprise a plurality of radial inlet ports disposed at different angular orientations around the valve stem and at different axial locations along the valve stem. The inlet selector valve cylinder may be oriented generally parallel to the pump cylinders. The inlet selector valve cylinder may comprise multiple inlet ports for connection to multiple fluid sources.

[0015] The identifying information may comprise at least one of a pump configuration/type number, a manufacturing batch number, a pump type identifier, a pump sequential identification number, or any combination thereof.

[0016] In yet another embodiment, the fluid pump device comprises a plurality of pump cylinders, a plunger reciprocally operable within each of the pump cylinders, each plunger comprising a piston interface member extending proximally therefrom that is split into at least two parts that are compressible towards one another, and an inlet selector valve to establish selective fluid communication between at least one fluid source and the pump cylinders. The inlet selector valve located may be laterally outboard of the pump cylinders.

[0017] The plungers may each comprise a distal end disc and a proximal end disc. The plungers may be reciprocally operable in the respective pump cylinders such that the distal end disc of each plunger is operable within a pumping zone of the pump cylinders and the proximal end disc is operable within an isolation zone of the pump cylinders. A seal may be provided at least circumferentially about each of the distal end disc and the proximal end disc.

[0018] A radial lip may be provided on each of the at least two parts of the piston interface member to interface with a drive piston. A support member may be coaxially disposed in the piston interface member. The radial lip on each of the at least two parts of the piston interface member may interface with a receiving groove defined in a socket in a drive piston. The piston interface member may be generally cylindrical shaped and the at least two parts may define at least two arcuate segments.

[0019] In another embodiment, a fluid delivery system is provided including a fluid pump device comprising a plurality of pump cylinders, a plunger reciprocally operable within each of the pump cylinders, and an inlet selector valve to establish selective fluid communication between at least one fluid source container and the pump cylinders, the inlet selector valve located laterally outboard of the pump cylinders. A drive and actuating system independently and reciprocally operates the plungers in the pump cylinders.

[0020] The inlet selector valve may be oriented generally parallel to the pump cylinders.

[0021] A pump manifold may control fluid communication to the pump cylinders, and the inlet selector valve may control fluid communication with the at least one fluid source to control fluid flow into the pump manifold. The pump manifold may comprise an inlet manifold channel and an outlet manifold channel, and the pump cylinders may each comprise at least one inlet opening for fluid communication with the inlet manifold channel and at least one outlet opening for fluid communication with the outlet manifold channel. The pump cylinders may be in selective fluid communication with the inlet manifold channel and the outlet manifold channel via respective inlet check valves and outlet check valves. The at least one outlet opening may be positioned at a high point in each of the pump cylinders for air bubble egress.

[0022] The inlet selector valve may comprise an inlet selector valve cylinder having a valve stem disposed therein, and the valve stem may define an axial passage and a plurality of radial inlet ports connected to the axial passage. The radial inlet ports may be disposed at different angular orientations around the valve stem. The valve stem may alternatively comprise a plurality of radial inlet ports disposed at different angular orientations around the valve stem and at different axial locations along the valve stem.

[0023] A saline manifold may be in selective fluid communication with the pump cylinders via the inlet selector valve to establish selective fluid communication between a saline fluid source and the pump cylinders. The saline manifold may extend across the plurality of pump cylinders. The inlet selector valve may be operable by the drive and actuating system independently of the plungers.

[0024] Identifying indicia may be provided on the fluid pump device and encoded with identifying information for the fluid pump device. The inlet selector valve may comprise an inlet selector valve cylinder having a valve stem disposed therein, and the identifying information may comprise at least an initial angular orientation of the valve stem in the inlet selector valve cylinder or a representation thereof. The valve stem may comprise a plurality of radial inlet ports. The radial inlet ports may be disposed at different angular orientations

around the valve stem. Alternatively, the radial inlet ports may be disposed at different angular orientations around the valve stem and at different axial locations along the valve stem. The inlet selector valve cylinder may be oriented generally parallel to the pump cylinders.

[0025] The identifying indicia may be an optically encoded transparent member. The identifying indicia may be disposed on one of the pump cylinders.

[0026] Each of the plungers may comprise a piston interface member extending proximally therefrom, and the piston interface member may be split into at least two parts that are compressible towards one another. The plungers may each comprise a distal end disc and a proximal end disc. The plungers may be reciprocally operable in the respective pump cylinders such that the distal end disc of each of the plungers is operable within a pumping zone of the pump cylinders and the proximal end disc is operable within an isolation zone of the pump cylinders. A seal may be provided at least circumferentially about each of the distal end disc and the proximal end disc. A radial lip may be provided on each of the at least two parts of the piston interface member to interface with a drive piston of the drive and actuating system. A support member may be coaxially disposed in the piston interface member.

[0027] A drive and actuating system may be provided for operating the fluid pump device. The drive and actuating system includes an extendable and retractable pump drawer to accept the fluid pump device, with the fluid pump device comprising a plurality of pump cylinders and a plunger reciprocally operable within each of the pump cylinders. Drive pistons are provided and adapted for mechanical connection to the plungers, respectively, to independently and reciprocally operate the plungers in the pump cylinders. Piston linear actuators are respectively coupled to the drive pistons, and drive motors are operatively coupled to the piston linear actuators, respectively, to provide motive forces to the piston linear actuators to independently and reciprocally operate the plungers.

[0028] The fluid pump device may further comprise an inlet selector valve to establish selective fluid communication between at least one fluid source container and the pump cylinders, and the inlet selector valve may be located laterally outboard of the pump cylinders.

[0029] An inlet selector valve actuator may be provided adapted for mechanical connection to the inlet selector valve to control operation of the inlet selector valve to establish the selective fluid communication between the at least one fluid source container and the pump cylinders.

[0030] A pump manifold may control fluid communication to the pump cylinders, and a pump clamping mechanism may be operable to secure the fluid pump device in the pump drawer and apply a compressive force to the pump manifold when the fluid pump device is loaded in the pump drawer. The pump clamping mechanism may comprise a clamping block to engage the pump manifold when the fluid pump device is loaded in the pump drawer. The clamping block may be operated by a clamp actuating mechanism to engage and disengage the clamping block with the pump manifold. The pump manifold may comprise a pressure sensing port with a pressure sensing diaphragm, and the drive and actuating system may further comprise a pressure measuring mechanism adapted to interface with the pressure sensing port. The operation of the clamp actuating mechanism to engage the clamping block with the pump manifold may concurrently cause the pressure measuring mechanism to operatively interface with the pressure sensing diaphragm. The drive and actuating system may further comprise a pressure measuring mechanism adapted to interface with the pressure sensing port.

[0031] The pump manifold may comprise an inlet manifold channel and an outlet manifold channel, and an outlet selector valve may be in fluid communication with the outlet manifold channel to control fluid flow from the pump manifold. The drive and actuating system may further comprise an outlet selector valve actuator to control operation of the outlet selector valve.

[0032] The plungers of the fluid pump device may each comprise a piston interface member split into at least two parts that are compressible towards one another to enable the mechanical connection with the respective drive pistons. A radial lip may be provided on each of the at least two parts to interface with the respective drive pistons. A support member may be coaxially disposed in the piston interface member. Further, a radial lip may be provided on each of the at least two parts of the respective piston interface members to interface with a receiving groove in a socket in the corresponding drive pistons of the drive and actuating system.

[0033] Another embodiment is directed to a method of interfacing a fluid pump device with a drive and actuating system of a fluid delivery system. The fluid pump device generally comprises a plurality of pump cylinders, and a plunger reciprocally operable within each of the pump cylinders, each of the plungers comprising a piston interface member extending proximally therefrom. The piston interface member is split into at least two parts that are compressible towards one another. The plungers are interfaced with respective drive pistons of the drive and actuating system, such that the at least two parts of each of the piston

interface members compress towards one another to enable mechanical engagement with the respective drive pistons. The drive pistons independently and reciprocally operate the plungers in the respective pump cylinders.

[0034] The fluid pump device may further comprise an inlet selector valve to establish selective fluid communication between at least one fluid source container and the pump cylinders, with the inlet selector valve located laterally outboard of the pump cylinders.

[0035] The plungers may each comprise a distal end disc and a proximal end disc. The plungers may be reciprocally operable in the respective pump cylinders such that the distal end disc of each of the plungers is operable within a pumping zone of the pump cylinders and the proximal end disc is operable within an isolation zone of the pump cylinders. A seal may be provided at least circumferentially about each of the distal end disc and the proximal end disc. A radial lip may be provided on each of the at least two parts of the respective piston interface members to interface with a receiving groove in a socket in the respective drive pistons of the drive and actuating system. A support member may be coaxially disposed in the piston interface member. In an alternative configuration, a radial lip may be provided on each of the at least two parts of the piston interface members, and the respective drive pistons may each comprise a distal end socket defining a receiving groove, such that the step of interfacing the plungers with the respective drive pistons comprises receiving the piston interface members into the distal end socket in the respective drive pistons and engaging the radial lip on the at least two parts with the receiving groove in the distal end socket in each of the respective drive pistons.

[0036] Another embodiment is directed to a method of assembling a fluid pump device, comprising providing a pump body having a plurality of pump cylinders and at least one inlet selector valve cylinder located laterally outboard of the pump cylinders, inserting an inlet selector valve body comprising a valve stem into the inlet selector valve cylinder such that the valve stem is in a predetermined angular orientation in the inlet selector valve cylinder, and inserting respective plungers into the pump cylinders.

[0037] The pump body may further comprise a saline manifold extending across the pump cylinders and defining at least one saline channel, and the method may further comprise installing a saline manifold cap onto the pump body to enclose the at least one saline channel.

[0038] The pump body may comprise a front plate and the pump cylinders may extend proximally from the front plate, and the method may further comprise installing a pump manifold plate onto the front plate to form a pump manifold. At least one check valve may be captured between the manifold plate and the front plate during the step of installing the

manifold plate onto the front plate to form the pump manifold. The front plate may comprise at least one inlet manifold channel defined by at least one channel member, and the method may further comprise installing an inlet manifold cap on the at least one channel member to enclose the at least one inlet manifold channel. The manifold plate may comprise an outlet selector valve cylinder, and the method may further comprise inserting an outlet selector valve body comprising a valve stem into the outlet selector valve cylinder. The outlet selector valve cylinder may comprise a patient outlet port and a waste outlet port and the valve stem of the outlet selector valve body defines a flow passage, and the step of inserting the outlet selector valve body into the outlet selector valve cylinder may comprise aligning the flow passage to be in fluid communication with the waste outlet port. The step of inserting the outlet selector valve body into the outlet selector valve cylinder may be preceded by spraying lubricant onto the interior wall surface of the outlet selector valve cylinder.

[0039] The method may further comprise spraying lubricant onto the interior wall surface of the pump cylinders and onto the interior surface of the at least one inlet selector valve cylinders prior to the steps of inserting the inlet selector valve body into the inlet selector valve cylinder and inserting the respective plungers into the pump cylinders.

[0040] The steps of inserting the inlet selector valve body into the inlet selector valve cylinder and inserting the respective plungers into the pump cylinders can occur concurrently.

[0041] The predetermined angular orientation of the valve stem of the inlet selector valve body may be encoded in identifying indicia provided on the pump body, and the identifying indicia may be a bar code.

[0042] The method may further comprise generating an inlet selector valve position number and encoding the inlet selector valve position number as identifying indicia provided on the pump body. The inlet selector valve position number may correspond to the predetermined angular orientation of the valve stem of the inlet selector valve body in the inlet selector valve cylinder. The method may further comprise etching the identifying indicia on one of the pump cylinders.

[0043] Further details and advantages of the various embodiments described in detail herein will become clear upon reviewing the following detailed description of the various embodiments in conjunction with the accompanying drawing figures.

BRIEF DESCRIPTION OF THE DRAWINGS

[0044] FIG. 1 is a schematic view of a fluid delivery system for continuous multi-fluid delivery applications.

[0045] FIG. 2 is a front perspective view of a fluid pump device for use in the fluid delivery system shown in FIG. 1.

- [0046] FIG. 3 is a rear perspective view of the fluid pump device shown in FIG. 2.
- [0047] FIG. 4 is a bottom perspective view of the fluid pump device shown in FIG. 2.
- [0048] FIG. 5A is a bottom view of the fluid pump device shown in FIG. 2.
- [0049] FIG. 5B is a detail view of detail 5B in FIG. 5A.
- [0050] FIG. 6 is an exploded perspective view of the fluid pump device shown in FIG. 2.
- [0051] FIG. 7 is a front perspective view of a pump body of the fluid pump device shown in FIG. 2.
- [0052] FIG. 8 is a rear perspective view of the pump body shown in FIG. 7.
- [0053] FIG. 9 is a rear view of a pump cylinder of the pump body shown in FIG. 7.
- [0054] FIG. 10 is a cross-sectional view of the fluid pump device taken along line 10-10 in
- FIG. 2 and with a plunger of the fluid pump device removed for clarity.
- [0055] FIG. 11 is a rear perspective view of a plunger for the fluid pump device shown in FIG. 2.
- [0056] FIG. 12 is a cross-sectional view taken along line 12-12 in FIG. 11.
- [0057] FIG. 13 is a cross-sectional perspective view of a distal portion of a drive piston adapted to capture and actuate the plunger shown in FIG. 11.
- [0058] FIG. 14 is a cross-sectional perspective view showing engagement of the drive piston shown in FIG. 13 with the plunger shown in FIG. 11.
- [0059] FIG. 15 is a perspective view of the fluid pump device showing inlet manifold caps exploded from the fluid pump device.
- [0060] FIG. 16 is a perspective view of a right front portion of a pump manifold plate adapted for association with the pump body shown in FIG. 7.
- [0061] FIG. 17 is a rear perspective view of the pump manifold plate supporting inlet and outlet check valves of the fluid pump device.
- [0062] FIG. 18 is a rear perspective view of a right portion of a pump manifold plate adapted for association with the pump body shown in FIG. 7.
- [0063] FIG. 19 is a longitudinal cross-sectional and perspective view of a portion of the pump manifold plate adapted for association with the pump body shown in FIG. 7.
- [0064] FIG. 20 is a cross-sectional perspective view of a portion of the fluid pump device shown in FIG. 2 showing operation of an inlet check valve of the fluid pump device.
- [0065] FIG. 21 is a cross-sectional perspective view of a portion of the fluid pump device shown in FIG. 2 showing operation of an outlet check valve of the fluid pump device.

[0066] FIG. 22 is a cross-sectional perspective view taken along line 22-22 in FIG. 17.

[0067] FIG. 23 is a cross-sectional perspective view taken along line 23-23 in FIG. 3.

[0068] FIG. 24A is an isometric perspective view of an outlet selector valve body used in the fluid pump device shown in FIG. 2.

[0069] FIG. 24B is a cross-sectional perspective view taken along line 24B-24B in FIG. 24A.

[0070] FIGS. 25A-25Q illustrate additional embodiments of the outlet selector valve wherein the outlet selector valve body is embodiment with different sealing arrangements.

[0071] FIG. 26 is an isometric perspective view of a swabable valve for use in association with the outlet selector valve shown in FIG. 24.

[0072] FIG. 27 is a cross-sectional perspective view taken along line 27-27 in FIG. 3.

[0073] FIG. 28A is an isometric front perspective view of an inlet selector valve stem used in the fluid pump device shown in FIG. 2.

[0074] FIG. 28B is an isometric rear perspective view of the inlet selector valve stem used in the fluid pump device shown in FIG. 2.

[0075] FIGS. 28C-28D are isometric perspective view of the inlet selector valve stem shown in FIGS. 28A-28B and further comprising a first exemplary sealing arrangement.

[0076] FIGS. 28E-28F are isometric perspective view of the inlet selector valve stem shown in FIGS. 28A-28B and further comprising a second exemplary sealing arrangement.

[0077] FIG. 29A-29H are schematic cross-sectional views of the inlet selector valve showing exemplary operation thereof.

[0078] FIG. 30 is a cross-sectional perspective view taken along line 30-30 in FIG. 3.

[0079] FIG. 31 is a cross-sectional perspective view of one of the pump cylinders of the fluid pump device of **FIG. 2** showing a forward-most position of the plunger disposed in the right inboard pump cylinder.

[0080] FIG. 32 is a horizontal cross-sectional and perspective view of a right side portion of the fluid pump device shown in FIG. 2 to show inflow from a first fluid source container associated with the fluid pump device.

[0081] FIG. 33 is a horizontal cross-sectional and perspective view of a right side portion of the fluid pump device shown in FIG. 2 to show inflow from a second fluid source container associated with the fluid pump device.

[0082] FIG. 34 is a horizontal cross-sectional and perspective view of a right side portion of the fluid pump device shown in FIG. 2 to show inflow from a right side saline source associated with the fluid pump device.

[0083] FIG. 35 is a horizontal cross-sectional and perspective view of a right side portion of the fluid pump device shown in FIG. 2 to show inflow from a left side saline source associated with the fluid pump device.

- [0084] FIG. 36 is an enlarged view of the cross-sectional perspective view shown in FIG. 35.
- [0085] FIG. 37 is a cross-sectional perspective view taken through a pump cylinder of the fluid pump device shown in FIG. 2, and showing an inlet check valve and an outlet check valve of the fluid pump device.
- [0086] FIG. 38 is a cross-sectional and perspective view that is an enlargement of a portion of the view shown in FIG. 37.
- [0087] FIG. 39 is a cross-sectional perspective view taken through the same pump cylinder shown in FIG. 37, and showing fluid flow in an outlet manifold channel of the fluid pump device.
- [0088] FIG. 40 is a schematic view showing the fluid pump device of FIG. 2 with a first or basic embodiment of a fluid supply set associated with the fluid pump device.
- [0089] FIG. 41 is a schematic view showing the fluid pump device of FIG. 2 with a second or high-use embodiment of the fluid supply set associated with the fluid pump device.
- [0090] FIG. 42 is a schematic view showing the fluid pump device of FIG. 2 with a third or limited-use embodiment of the fluid supply set associated with the fluid pump device.
- [0091] FIG. 43 is a schematic view showing the fluid pump device of FIG. 2 with a fourth and additional limited-use embodiment of the fluid supply set associated with the fluid pump device that may be used with single-patient fluid source containers.
- [0092] FIG. 44 is a perspective view of an exemplary patient supply set for use with the fluid pump device shown in FIG. 2.
- [0093] FIG. 45 is a schematic view showing the fluid pump device with the second or high-use embodiment of the fluid supply set as shown in FIG. 41, and further showing a waste collection system associated with the fluid pump device.
- **[0094] FIG. 46A** is a perspective view of the fluid delivery system for continuous multifluid delivery applications embodied as a mobile system.
- [0095] FIG. 46B is a schematic view of the fluid delivery system of FIG. 46A shown interfacing with external devices including a remotely located display, computed tomography scanner, and a computer network as examples.

[0096] FIG. 47 is a schematic representation of a drive and actuating system for the fluid delivery system shown in **FIG. 46A**, and further showing features of a control system for the fluid delivery system.

[0097] FIG. 48 is a top perspective of the drive and actuating system for the fluid delivery system shown in **FIG. 46A**, with a pump drawer in a closed position.

[0098] FIG. 49 is a top perspective view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, with the pump drawer in an open position.

[0099] FIG. 50 is a side perspective view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, with the pump drawer in the open position.

[00100] FIG. 51 is a side view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, with the pump drawer in the closed position.

[00101] FIG. 52 is a top view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, with the pump drawer in the closed position.

[00102] FIG. 53 is a cross-sectional view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, taken along line 53-53 in FIG. 52.

[00103] FIG. 54 is a cross-sectional view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, taken along line 54-54 in FIG. 52.

[00104] FIG. 55 is a top perspective view of a rear portion of the drive and actuating system for the fluid delivery system shown in FIG. 46A.

[00105] FIG. 56 is a front perspective view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, with the pump drawer in the closed position.

[00106] FIG. 57 is a top perspective view of a front portion of the drive and actuating system for the fluid delivery system shown in FIG. 46A.

[00107] FIG. 58 is a cross-sectional view of the drive and actuating system for the fluid delivery system shown in FIG. 46A, taken along line 58-58 in FIG. 52.

[00108] FIG. 59 is a top view of a pressure measurement mechanism for the fluid delivery system shown in FIG. 46A.

[00109] FIG. 60 is a perspective view of a fluid handling compartment provided in the mobile fluid delivery system shown in FIG. 46A.

[00110] FIG. 61 is a velocity vs. time graph illustrating velocity profiles under typical operating conditions for a two (2) plunger – pump cylinder arrangement.

[00111] FIG. 62 is a flow rate vs. time graph corresponding to the two (2) plunger – pump cylinder arrangement of FIG. 61.

[00112] FIG. 63 is a perspective view of a drive piston incorporating a force transducer for use in detecting an under volume condition during the course of a fluid injection.

[00113] FIG. 64 is a force vs. displacement graph illustrating a potential use of the drive piston shown in FIG. 63.

[00114] FIG. 65 is a velocity vs. time graph illustrating velocity profiles during a slight under volume operating condition for a second plunger – cylinder combination in a two (2) plunger – pump cylinder arrangement.

[00115] FIG. 66 is a flow rate vs. time graph showing the combined output flow rate for the two (2) plunger – cylinder arrangement of FIG. 65.

[00116] FIG. 67 is a flow rate vs. time graph showing the combined output flow rate for a two (2) plunger – cylinder arrangement in which the second plunger – cylinder combination experiences a severe under volume operating condition.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

[00117] For purposes of the description hereinafter, spatial orientation terms, as used, shall relate to the referenced embodiment as it is oriented in the accompanying drawing figures or otherwise described in the following detailed description. However, it is to be understood that the embodiments described hereinafter may assume many alternative variations and configurations. It is also to be understood that the specific components, devices, features, and operational sequences illustrated in the accompanying drawing figures and described herein are simply exemplary and should not be considered as limiting.

[00118] Referring initially to FIGS. 1-6, a fluid pump device 10, generally provided in the form of a disposable pump cassette, is shown. While fluid pump device or pump cassette 10 (hereinafter referred to as "pump 10") is intended as a disposable component, the pump 10 is intended for multiple uses prior to disposal. Such multiple uses may be for multiple patients or for a multiple and discrete number of uses in medical diagnostic and therapeutic procedures which may involve a single or multiple patients. The pump 10 is adapted to interface with a drive and actuating system 400 that accepts, drives, and actuates various components on the pump 10. The drive and actuating system 400 is described herein in connection with FIGS. 46-60. A control system 800 is also provided to control operation of the various components of the drive and actuating system 800, as described herein in connection with FIGS. 46-60.

[00119] The pump 10 may be considered to have a front or distal side 12, a rear or proximal side 14, a right side 16 as viewed looking from the front or distal side 12 toward the

toward the rear or proximal side 14, and a left side 18 as viewed looking from the front or distal side 12 toward the rear or proximal side 14. Generally, as shown schematically in FIG. 1, the pump 10 may be part of a fluid delivery system 2 which includes the drive and actuating system 400, discussed herein. The pump 10 generally comprises a fluid supply section 20, a pump metering and pressurizing section 22, and a pump outlet section 24. The fluid supply section 20 includes one or more fluid source containers 30 containing various fluids to be supplied to the pump 10, and a fluid supply set 32 (see FIGS. 40-43 discussed herein) that conducts the one or more fluids to the pump 10. Various versions and embodiments of the fluid supply set 32 may be associated with the pump 10 to meet different patient and/or procedural needs, as described herein. Each of the various versions and embodiments of the fluid supply set 32 comprises one or more fluid supply tubes 34 each having one end connected to the pump 10 and the opposing end connected to a spike 36 used to access a fluid source container 30.

[00120] The pump outlet section 24 includes a disposable single-use or single-patient supply set 40 (hereinafter "patient supply set 40"; see FIG. 44 discussed herein) comprising medical tubing having opposed free ends each having a fluid connector 42 used to make a fluid connection, such as to a catheter inserted into a patient to convey a desired fluid or mixture of fluids to a desired location within a patient's body. At least one of the fluid connectors 42 may include a check valve (not shown) to prevent reverse flow from the patient. Additionally, the pump outlet section 24 comprises a waste collection system 44 that is associated with the pump 10 to collect and store waste fluids. The waste collection system 44 generally comprises a waste collection tube set 46 connected to a waste collection container 48, as shown in FIG. 45 discussed further herein. The waste collection tube set 46 is adapted to make a fluid connection with the pump 10.

[00121] The pump 10 forms a part of the pump metering and pressurizing section 22. The pump 10 generally comprises a pump manifold 80, a pump body 100, a plurality of independently operable plungers 200 operatively associated with the pump body 100, a pump manifold plate 230 which is joined to the pump body 100 to form the pump manifold 80, an outlet selector valve 280 associated with the pump body 100 for controlling fluid delivery or output from the pump 10, and a plurality of inlet selector valves 300 associated with the pump body 100 for controlling fluid flow to the pump body 100. In operation, the pump 10 is typically interfaced with multiple and different fluids contained in the fluid source containers 30, and is actuated or operated by the drive and actuating system 400 to select a fluid type from the several fluid source containers 30 and continuously deliver fluids, either individually or as a fluid mixture, to the patient. The pump 10, under the directed operation of

the drive and actuating system **400**, draws in fluid directly from the fluid source containers **30** and accurately meters the appropriate volumes and specified fluid flow rates and infusion time to the patient via the patient supply set **40** (shown in **FIG. 44**). As noted in the foregoing, various fluid supply sets **32** may be associated with the pump **10** to meet different patient and/or procedural needs, and these various versions or embodiments are detailed further herein in connection with **FIGS. 40-43**.

[00122] The drive and actuating system 400 which operates the pump 10 pressurizes the fluid dispensed from the pump 10 to the patient supply set 40 sufficiently to overcome any resistance through the patient supply set 40 and the catheter connected thereto so that accurate fluid volume and pressure are delivered to the desired treatment or diagnostic location within the patient's body. Fluid flow from the pump 10 is delivered substantially continuously to the patient via an indwelling catheter and may be a single fluid, or multiple fluids delivered substantially simultaneously that are combined into a mixture of any desired proportions and delivered as a single stream via the outlet selector valve 280.

Referring additionally to **FIGS. 7-10**, the pump body **100** is typically formed as an integral or singular body formed from polycarbonate and like polymeric materials via an injection molding process. The pump body 100 comprises a front or distal plate 102 and a plurality of pump cylinders 104 extending proximally from the front plate 102. In the illustrated embodiment, a total of four (4) pump cylinders 104 are provided in the pump 10, with the two (2) right side pump cylinders 104 providing one fluid circuit and the two (2) left side pump cylinders 104 providing a second fluid circuit, as described in further detail herein. While of four (4) pump cylinders 104 are provided in the pump 10, the pump 10 may be "scalable" to include additional pairs of pump cylinders 104 or may be provided with just two (2) tandem pump cylinders 104. While the pump cylinders 104 are preferred to have a cylindrical shape, they may also have other symmetrical or non-symmetrical cross-sectional shapes (such as D-shaped) in vertical or transverse cross-section. Each pump cylinder 104 defines a pump chamber 106 and accepts a plunger 200 which is reciprocally operable within the pump cylinder 104. The plungers 200 are independently operable by the drive and actuating system 400. The respective pump cylinders 104 each have an interior wall or surface 108 that defines the pump chamber 106. The pump cylinders 104 each have a generally enclosed front or distal end wall 110 formed by the front plate 102 and an open rear or proximal end 112.

[00124] Additionally, the pump body 100 comprises a plurality of inlet selector valve cylinders 114 that extend proximally from the front plate 102 laterally outboard of the two (2)

chamber 116 that accepts an inlet selector valve 300 which is rotationally operable within the inlet selector valve cylinder 114. The drive and actuating system 400 also independently operates the respective inlet selector valves 300 disposed within the inlet selector valve cylinders 114. In the illustrated embodiment, two (2) inlet selector valve cylinders 114 are provided in pump 10 to respectively control inflow to the two (2) "right side" pump cylinders 104 providing one fluid circuit and the two (2) "left side" pump cylinders 104 providing the second fluid circuit in pump 10. The respective inlet selector valve cylinders 114 have a front or distal end opening 118 formed in the front plate 102 and a rear or proximal end opening 120 to accept the inlet selector valve 300.

Each inlet selector valve cylinder 114 comprises, in the illustrated embodiment, a [00125] pair of inlet ports 122, 124 for use in connecting the pump 10 to two (2) fluid sources of diagnostic or therapeutic (e.g., pharmaceutical) fluids, such as imaging contrast media, to be received in the pump chambers 106 of the pump cylinders 104. Further, each inlet selector valve cylinder 114 comprises, in the illustrated embodiment, an additional rear or proximal inlet port 126 for use in connecting the pump 10 to, typically, a source of flushing or diluting fluid such as saline. As such, the rearmost inlet port 126 is referred to hereinafter as a "saline port 126", while inlet ports 122, 124 are referred to hereinafter as "first and second inlet ports 122, 124", respectively. The inlet ports 122, 124, 126 are axially spaced along the inlet selector valve cylinder 114, with the first inlet port 122 located near the front plate 102 and the saline port 126 located near the rear or proximal end opening 120 of the inlet selector valve cylinder 114. The saline port 126 is located at a lower level than the first and second inlet ports 122, 124, and connects to a saline manifold located on the underside of the pump body 100, as described herein. Accordingly, the saline port 126 is located at a lower level and opens into the inlet selector valve cylinder 114 and the saline manifold 130 to access one of two (2) saline channels in the saline manifold 130, as described herein, rather than intersecting or directly opposing the valve body of the inlet selector valve 300 as in the case of the first and second inlet ports 122, 124. The first and second inlet ports 122, 124 and the saline ports 126 on the inlet selector valve cylinders 114 may be formed with luer-type connector tips or barbed connection tips, and like fluid connections arrangements, for making either removable or permanent fluid connections to the fluid supply tubes 34 used to connect the pump 10 to the one or more fluid source containers 30 that provide therapeutic or diagnostic (e.g., pharmaceutical) fluids or saline to the pump 10.

[00126] The illustrated embodiment of the pump 10 is shown for exemplary purposes with six (6) supply ports, three (3) on each of the right and left sides 16, 18 of the pump 10. These supply ports include the two (2) right side inlet ports 122, 124 and the right side saline port 126 on the pump body 100 and the two (2) left side inlet ports 122, 124 and the left side saline port 126 on the pump body 100. However, this specific configuration is illustrated for expediency in explaining the various components, features, and desirable operational characteristics of the pump 10 and should be considered as non-limiting. Accordingly, the pump 10 may comprise a fewer or a greater number of ports 122, 124, 126 on each side 16, 18, as desired.

The saline port 126 on the respective inlet selector valve cylinders 114 is in fluid communication with a saline manifold 130 that extends across the underside of the pump body 100 and across the pump cylinders 104. The saline manifold 130 is oriented generally parallel to the front plate 102. The saline manifold 130 is typically adapted to be placed in fluid communication via the two (2) saline ports 126 to two (2) sources of saline S1, S2 contained in two (2) respective fluid source containers 30. The saline manifold 130 is bifurcated into two (2) saline channels 132, 134. The respective inlet selector valves 300 are configured so that saline may be drawn from either of the sources of S1, S2 in the saline fluid source containers 30 via the saline channels 132, 134, even though the saline fluid source container 30 may be physically on the opposite side of the pump 10 from the inlet selector valve 300, as described further herein. In the illustrated embodiment of the pump 10, the forward or distal or "first" saline channel 132 of the saline manifold 130 is supplied by the saline source S2 in the fluid source container 30 connected to the saline port 126 located on the right side inlet selector valve cylinder 114, and the rear or proximal or "second" saline channel 134 of the saline manifold 130 is supplied by the saline source S1 in the fluid source container 30 connected to the saline port 126 located on the left side inlet selector valve cylinder 114. The shape of the saline channels 132, 134 may be formed with smooth interior surfaces and curvatures to minimize the potential for trapped air and pressure drop (e.g., flow restriction) through each saline channel 132, 134. A saline manifold cap 136 encloses the saline channels 132, 134 and may be secured in place on the saline manifold 130 formed on the underside of the pump body 100 via medical grade adhesive, solvent bonding, laser and ultrasonic welding, and like joining techniques.

[00128] As the forward saline channel 132 is connected to the right saline source S2 and the rear saline channel 134 is connected to the left saline source S1, it is desirable to purge air using saline from the left saline source S1 as this is the rearmost saline channel. By using the

rearmost saline channel 134 connected to the left saline source S1 for fluid priming operations, the fluid passages in the pump 10 may be primed from rear to front with saline, and air is purged forward from the rear of each of the inlet selector valves 300. This result occurs because there are no other ports "behind" the rearmost saline channel 134. For example, it would not be possible to purge all of the air from the inlet selector valves 300 if one of the inlet ports 122, 124 was used to supply a priming fluid. This is because there would be a "dead space" in the inlet selector valve 300 behind the two (2) front inlet ports 122, 124 through which no fluid would flow. Any air in this portion of the inlet selector valve 300 would remain after priming.

A front or distal side **140** of the front plate **102** defines a plurality of inlet openings 142, one for each of the pump cylinders 104. The inlet openings 142 are provided in the distal end wall 110 of each of the pump cylinders 104. The inlet openings 142 permit fluid to enter the pump chamber 106 of the respective pump cylinders 104. The inlet openings 142 are spaced apart on the front plate 102 to respectively coincide with the pump chambers 106 of the respective pump cylinders 104. Accordingly, four (4) spaced inlet openings 142 are provided in the illustrated embodiment, one for each pump cylinder 104, and are positioned to be near the bottom center of each of the pump cylinders 104, as shown in FIG. 9. An inlet check valve support structure 144 is provided in each of the inlet openings 142 and is desirably recessed within each of the inlet openings 142 for supporting an inlet check valve 194. The inlet check valves 194 are flexible polymeric, typically polyurethane, disks that regulate the fluid flow into each pump cylinder 104. The inlet check valve support structure 144 comprises a central hub 146 and one or more prongs 148 extending radially outward from the central hub 146. A total of three (3) prongs 148 is present in the inlet check valve support structure 144 in the illustrated embodiment. The central hub 146 desirably includes a centrally-located preload pin 150 that allows a preload force to be applied to the inlet check valve 194 to ensure that the inlet check valve 194 closes when there is no pressure gradient present across the inlet check valve 194. The preload force is not set too high so as to overly increase the "cracking" or opening pressure of the inlet check valve 194 as this would undesirably cause a higher pressure drop across the check valve 194. The preload pins 150 also help to counteract the effects of long-term storage, which could cause the inlet check valves 194 to develop a compression set over time. The front or distal end openings 118 in the front plate 102 leading to the inlet selector valve cylinders 114 are circumferentially bordered by one or more concentric ribs or rims 152 formed on the front side 140 of the front plate 102 and which extend around the front or distal end openings 118.

The front side 140 of the front plate 102 further defines an elongated recess 154 [00130] extending across the front side 140 above the elevational location of the inlet openings 142, but still coinciding with the pump chambers 106 of the respective pump cylinders 104. The elongated recess 154 is bordered by a perimetrical recess 156 so that a sealing element, such as an elongated O-ring or gasket or like sealing element, may be placed in the perimetrical recess 156 and form a fluid sealing border about the elongated recess 154. A plurality of recessed areas 158 is defined in the elongated recess 154 and is spaced apart in the elongated recess 154 to coincide, respectively, with the pump chamber 106 defined by the pump cylinders 104. Accordingly, a total of four (4) recessed areas 158 is provided in the illustrated embodiment. Each recessed area 158 typically defines at least one top or air egress opening 160 in the distal end wall 110 of each of the pump cylinders 104, and is desirably positioned to be near the top center of each of the pump cylinders 104, as shown in FIG. 9, for providing an egress opening for air bubbles in the pump chambers 106 of the respective pump cylinders 104. Each of the recessed areas 158 further defines one or more outlet openings 162 in the front plate 102, typically on either side of the top air egress opening 160, and in the distal end wall 110 of each of the pump cylinders 104 to permit fluid to exit the respective pump cylinders 104. It is also noted that the upper surface or leg of the elongated recess 154 is substantially flat and horizontal and its centerline is raised slightly above the recessed areas 158 which allows any air that is present in the elongated recess 154 to be ejected upward through the outlet selector valve 280.

[00131] In summary, each pump cylinder 104 has an inlet opening 142 in fluid communication with its pump chamber 106 and one or more outlet openings 162 in fluid communication with its pump chamber 106, with the one or more outlet openings 162 defined in one of the recessed areas 158 in the elongated recess 154 defined in the front side 140 of the front plate 102. Referring next to FIG. 10, the pump cylinder 104 generally has a working or pumping region or zone identified by arrow 164 in the pump chamber 106 and an isolation region or zone identified by arrow 166 in the pump chamber 106. The plunger 200 is removed in the view of FIG. 10 for clarity.

[00132] A plate support structure or groove 168 may be provided on at least one of the pump cylinders 104, such as provided on a top or upper facing side of one of the outboard pump cylinders 104. The plate support structure 168 supports a pump indicator plate 170 which is encoded with identifying information regarding the pump 10 to enable the control system 800 which controls operation of the drive and actuating system 400 to determine, for example, the configuration of the pump 10. The configuration of the pump 10 is dependent,

typically, on the type or configuration of the fluid supply set **32** as manufactured or associated with the pump **10** and used to meet different patient and/or procedural needs.

The configuration of the pump 10 may also, or alternatively, be encoded into identifying indicia 172, such as bar code indicia as shown in FIG. 2, that is affixed on or etched into a top or upper facing side of one of the pump cylinders 104, such as affixed on or etched into the opposite outboard pump cylinder 104 from the pump cylinder 104 carrying the pump indicator plate 170. It will be understood that the pump indicator plate 170 and identifying indicia 172 may be located on any suitable surface or location on the pump body 100 or on the pump manifold plate 230. The identifying indicia 172 may also be a suitable RFID (radio frequency identification device) tag, as shown in FIG. 3, as a suitable arrangement for storing pertinent information about the pump 10. The identifying indicia 172 is scanned prior to installation of the pump 10 in association with the drive and actuating system 400 to determine the configuration of the pump 10, and other identifying information. The pump indicator plate 170 and/or the identifying indicia 172 may contain additional pertinent information, such as pump serial number, manufacturing identification number, useby date, manufacturing lot code/batch number, initial angular orientation of the inlet selector valves 300 in their respective inlet selector valve cylinders 114 on the pump body 100, cryptographic hash code to confirm validity of information, and like information. More limited information may be carried by the pump indicator plate 170 than the identifying indicia 172, with the identifying indicia 172 typically including all of the foregoing information. Thus, the pump indicator plate 170 may alternatively be encoded with only limited information, such as pump type information to identify the specific configuration of the pump 10 as shown, for example, in FIGS. 40-43 discussed herein. Moreover, if the identifying indicia 172 is an RFID (radio frequency identification device) tag, the RFID tag or device can store the same information listed above, such as: pump type/configuration, pump serial number, manufacturing identification number, use-by date, manufacturing lot code/batch number, and initial angular orientation of the inlet selector valves 300 in their respective inlet selector valve cylinders 114 on the pump body 100. Because RFID tags can have read/write capability, the RFID tag could also store information on how many times the "tagged" pump 10 has been used, the volume of pumped fluid, peak pressure, and like operational information. The RFID tag may be located on any suitable surface of the pump 10 and can be read and written to by an antenna in close proximity to the pump 10, such as associated with the drive and actuating system 400.

[00134] The pump indicator plate 170 is typically provided as an optically encoded transparent polymeric member that fits within and is secured by the plate support structure 168. The indicator plate 170 provides a length of material disposed along at least a portion of the wall. The length of material propogates electromagnetic energy therethrough. The length of material may include at least two indicators or grooves 174, each of the grooves being located at a different predetermined longitudinal position along the length of material and each of the grooves being positioned to longitudinally align with a sensor when a barrel, such as one of the pump cylinders 104, is engaged with the drive and actuating system 400 and thereby attached to the fluid injector portion of the fluid delivery system 2. The pump indicator plate 170 comprises a series of grooves 174 that permits at least the configuration of the pump 10 to be optically read or verified after installation in association with the drive and actuating system 400. Thus, the drive and actuating system 400 may include an optical detector and like technology and the pump indicator plate 170 may be provided and encoded with information in accordance with the disclosures of United States Patent Nos. 7,018,363 and 7,462,166, both to Cowan et al., which disclose optical technology for determining configuration, including size of a fluid pumping component mounted to a power fluid injector and are incorporated herein by reference in their entirety for these and any other pertinent applications. The foregoing Cowan patents are generally directed to syringes and like pump devices such that the optical technology therein may be applied to the pump cylinders 104 of the pump 10. The pump cylinders 104 are analogous and operable generally in the same manner as cylindrical syringe bodies and like pump devices as disclosed in the foregoing Cowan patents. Thus, the optical technology described in the foregoing Cowan patents may be applied to the pump cylinders 104 whereby the pump indicator plate 170 is provided with the optical technology detailed in these patents or the pump cylinders 104 are marked or otherwise identified in the various manners and embodiments disclosed in these patents. The pump indicator plate 170 is provided as an exemplary element for applying the indentifying indicia 172 to the pump 10 and should not be deemed limiting as this application expressly includes application of the optical technology found in the foregoing Cowan patents to the pump 10 generally and the pump body 100 in particular. The pump body 100 may be opaque to absorb laser light during a laser welding process during assembly of the pump 10, but the opaque pump body 100 also helps with optical sensor performance in the optical reading of the information contained in the grooves 174 in the pump indicator plate 170. Additionally, the plate support structure 168 may be adapted for a snap-lock fit with the pump indicator plate 170. The plate support structure 168 may comprise a recessed groove 176 in the pump

cylinder 104 for accepting the pump indicator plate 170, and a pair of flanges 178 for restraining the pump indicator plate 170 in the groove 176. Further, the snap-lock fit may be provided by a snap-lock tab 180 formed within the groove 176 in the pump cylinder 104 and a corresponding mating recess (not shown) defined in the underside of the pump indicator plate 170.

Referring further to FIGS. 11-14, as noted previously, a plunger 200 is [00135] reciprocally operable within each of the pump cylinders 104 and is independently controlled by the drive and actuating system 400. Each plunger 200 comprises a rigid plunger body 202 that is injection molded from polycarbonate and like polymeric materials. The plunger body 202 may be a unitary, solid body formed to include a series of wall segments 204 that extend between a front or distal end disc 206 and a rear or proximal end disc 208. The rear or proximal end disc 208 is formed with a piston interface member or device 210 which is adapted to interface with an independent drive piston 50 associated with the drive and actuating system 400 for the pump 10. The piston interface member 210 is split into at least two (2) parts or halves to form opposing halves or legs 212 that may compress towards one another, or radially inward toward a central longitudinal axis of the plunger 200, to be received in a distal end recess or socket 52 in the drive piston 50. Additionally, the piston interface member 210 comprises a circumferential radial lip or rim 214, which is provided on each of the interface halves or legs 212, to engage a corresponding groove or recess 53 defined proximally inward from radial lip or rim 54 provided in the distal end socket 52 in the drive piston 50. The engaging lips or rims 54, 214 secure the engagement between the plunger 200 and drive piston 50. Thus, the rear or proximal end disc 208 of each plunger body 202 includes several features that allow the plunger 200 to "snap" into the distal end socket 52 in the actuating drive piston 50. A desirable result of the foregoing "snap-fit" connection is that it is non-orientation specific and the drive piston 50 may engage the plunger **200** in any radial orientation of the plunger **200**. Moreover, it will be understood that the piston interface member 210 may be split into a plurality of portions or parts 212 that may compress inwardly toward a central longitudinal axis of the plunger 200. Additionally, the piston interface member 210 may be generally cylindrical shaped and, as such, the plurality of portions or parts may be formed as arcuate sections or segments.

[00136] Once the plunger 200 is "snapped" into place in association with the drive piston 50, the drive piston 50 can move the plunger 200 in a reciprocal manner in the associated pump cylinder 104. When the plunger 200 is pressurizing fluid in the pump chamber 106 of the pump cylinder 104 by moving forward or distally in the pump cylinder 104, a central ring

seats against a flat interior end or bottom 56 of the distal end socket 52 in the actuating drive piston 50, thereby transferring the compressive axial load to the drive piston 50. The support member 216 coaxially disposed in the piston interface member 212. When the pump 10 is to be removed from the drive and actuating system 400, the drive piston 50 is retracted rearward or proximally until the rear or proximal end disc 208 of the plunger body 202 contacts a stationary projection. Further retraction of the drive piston 50 disengages the snap-fit interface between the piston interface member 210 and the drive piston 50.

Each plunger 200 comprises two (2) over-molded seals, a front or distal end lip seal 218 provided circumferentially about and on the front side of the front or distal end disc 206, and a rear or proximal bead seal 220 provided circumferentially about the rear or proximal end disc 208. The front end disc 206 with over-molded lip seal 218 is used to seal liquid within the pumping zone 164 of the pump cylinder 104, and the rear end disc 208 with over-molded bead seal 220 is used to prevent wetted portions of the interior wall 108 of the pump cylinder 104 from being exposed to the ambient environment. The seals 218, 220 may be made of polyurethane and like polymeric materials. The front lip seal 218 is desirably adapted to withstand fluid pressure of at least 400 psi and, desirably, at least 500 psi and is desirably hydraulically energized by fluid pressure. Accordingly, higher pressures result in greater sealing force. The rear bead seal 220 typically seals against dust and particulates that may be pulled into the open rear or proximal end 112 of the pump cylinder 104, and is actuated by compression within the isolation zone 166 of the pump cylinder 104. Seal runners 222 may extend from the front lip seal 218 to the rear bead seal 220 along two (2) or more or all of the wall segments 204. In the illustrated embodiment, seal runners 222 extend along two (2) of the wall segments 204 located on opposite lateral sides of the plunger body 202. The seal runners 222 are typically formed during the over-molding process used to form the front lip seal 218 and the rear bead seal 220 on the front and rear end discs 206, 208, respectively. The "flat" front of the front end disc 206 is desirable for minimizing residual fluid volume in the pump chamber 106 of the pump cylinder 104, helps to eject air bubbles from the pump chamber 106 during fluid priming of the pump 10 and, further, helps clean the pump chamber 106 during flushing procedures.

[00138] It is noted that the retaining force of the snap-fit connection between the drive piston 50 and the plunger 200 is significantly greater than the expected retraction force to be applied to the plunger 200. The expected retraction force is the sum of the vacuum/suction force on the plunger 200 during filling of the pump cylinder 104 and the friction between the

foregoing plunger seals **218**, **220** and the interior wall **108** of the pump cylinder **104**. If snap-fit retention force is too low, the plunger **200** could disconnect prematurely from the drive piston **50** during use.

[00139] Referring additionally to FIGS. 15-19, the pump 10, as noted previously, comprises a pump manifold 80 that is formed by the connection or joining of the pump manifold plate 230 with the pump body 100. The pump manifold 80 is generally formed by assembling the pump manifold plate 230 to front plate 102 of the pump body 100. The pump manifold plate 230 (hereinafter "manifold plate 230") comprises a front or distal side 232 and a rear or proximal side 234. The manifold plate 230 is generally shaped to correspond to the shape of the front plate 102 of the pump body 100 and is joined with the front plate 102 so that the rear side 234 of the manifold plate 230 is in engagement with the front side 140 of the front plate 102. The front side 232 of the manifold plate 230 includes right and left inlet manifold channels 236 provided on lateral right and left halves of the manifold plate 230. The inlet manifold channels 236 generally extend longitudinally along the front side 232 of the manifold plate 230. The two inlet manifold channels 236 correspond, respectively, to the two (2) right side pump cylinders 104 and the two (2) left side pump cylinders 104 of the pump body 100. As noted previously, in the illustrated embodiment, a total of four (4) pump cylinders 104 is provided in pump 10, with the two (2) "right" side pump cylinders 104 providing one fluid circuit and the two (2) "left" side pump cylinders 104 providing a second fluid circuit. The "right" inlet manifold channel 236 corresponds to the two (2) "right" side pump cylinders 104, and the "left" inlet manifold channel 236 corresponds to the two (2) "left" side pump cylinders 104. Alignment slots or holes 237 may be provided in the manifold plate 230 to facilitate loading of the pump 10 in association with the drive and actuating system 400, which is described herein.

[00140] Each of the right and left inlet manifold channels 236 is defined by a raised channel member or flange wall 238 provided on the front side 232 of the manifold plate 230. The manifold plate 230 defines a lateral opening 240 in each of the inlet manifold channels 236 that coincides with the distal or front end opening 118 in the front plate 102 of the pump body 100 which leads to the inlet selector valve cylinder 114. Accordingly, each lateral opening 240 registers with a corresponding front end opening 118 to place the "right" and "left" inlet selector valves 300 in fluid communication with the corresponding "right" and "left" inlet manifold channels 236, respectively. Additionally, the manifold plate 230 defines two (2) sets of inlet openings 242 in each of the right and left inlet manifold channels 236 that correspond to the inlet openings 142 in the front plate 102 of the pump body 100. As noted

previously, the inlet openings 142 are spaced apart on the front plate 102 to respectively coincide with the pump chambers 106 of the respective pump cylinders 104, and the inlet openings 142 are positioned to be near the bottom center of each of the pump cylinders 104, as shown in FIG. 9. The respective sets of inlet openings 242 are, desirably, a plurality of openings 242 arranged in a predetermined pattern, such as a circular pattern, and enable fluid communication with the inlet openings 142 in the front plate 102 of the pump body 100. However, the two (2) sets of inlet openings 242 in each inlet manifold channel 236 may alternatively be provided as two (2) singular large openings in the respective inlet manifold channels 236. The illustrated circular arrangement of the inlet openings 242 desirably includes at least one inlet opening 242 located at a "high" point, such as near to the top part of the channel member 238 defining the inlet manifold channel 236. This "high point" inlet opening 242 minimizes the potential for air bubbles to become trapped within the inlet manifold channels 236 because any air present in the inlet manifold channels 236 is pulled into the pump cylinders 104 during the initial fluid priming process for the pump 10. The number and size of inlet openings 242 may be selected to minimize pressure drop across the underlying inlet check valves 194 during filling of the pump cylinders 104, while minimizing the potential for high pressures in the pump cylinders 104 which could cause the polymeric material of the inlet check valves 194 to "extrude" into the inlet openings 242 under high pressure.

[00141] The rear or proximal side 234 of the manifold plate 230 also defines an elongated outlet manifold channel or recess 244 extending across the rear side 234 above the elevational location of the sets of inlet openings 242 in the manifold plate 230, but still coinciding with or corresponding to the pump chambers 106 of the respective pump cylinders 104. The outlet manifold channel 244 generally corresponds to the elongated recess 154 defined in the front side 140 of the front plate 102 of the pump body 100. The elongated recess 154 is sized larger than the outlet manifold channel 244 and is bordered by the perimetrical recess 156, as described previously, so that an elongated O-ring or gasket and the like, may be placed in the perimetrical recess 156 and form a fluid sealing border around the outlet manifold channel 244 when the manifold plate 230 is joined to the front plate 102 of the pump body 100 to form the pump manifold 80. In a variation of the foregoing sealing arrangement, a weld joint, typically a laser weld, occupies the location of the perimetrical recess 156 and the sealing O-ring or gasket is not required, and this embodiment or variation is illustrated in the accompanying figures. The elongated recess 154 also forms the back wall of the outlet

manifold channel **244** when the manifold plate **230** is joined to the front plate **102** of the pump body **100**.

[00142] The outlet manifold channel 244 is used to place the respective pump cylinders 104 in fluid communication with the outlet selector valve 280 on the manifold plate 230. A plurality of outlet check valve receiving recesses 246 is defined as part of the outlet manifold channel 244. The outlet check valve receiving recesses 246 are spaced apart in the outlet manifold channel 244. Each of the receiving recesses 246 accommodates an outlet check valve 196. Thus, an outlet check valve receiving recess 246 is provided for each of the pump cylinders 104 of the pump body 100 so that an outlet check valve 196 opposes each of the respective sets of air egress openings 160 and outlet openings 162 in the front plate 102 of the pump body 100. The outlet check valve receiving recesses 246 are located directly above the sets of inlet openings 242 defined in the manifold plate 230, respectively. Each of the outlet check valve receiving recesses 246 further includes a centrally located preload pin 250 that allows a preload force to be applied to the outlet check valve 196 to ensure that the outlet check valve 196 closes when there is no pressure gradient present across the outlet check valve 196. The outlet check valves 196 are flexible polymeric discs, typically polyurethane discs, which regulate the fluid flow from each pump cylinder 104. Thus, the outlet check valves 196 are located within the respective outlet check valve receiving recesses 246 in the outlet manifold channel 244, with each of the outlet check valves 196 associated, respectively, with a corresponding set of outlet openings 162 and top openings 160 in the front plate 102 leading to the pump chambers 106 of the pump cylinders 104.

[00143] The rear or proximal side 234 of the manifold plate 230 further comprises dish-shaped areas or recesses 252 opposite the inlet openings 142 in the front plate 102 leading to the pump chambers 106 of the pump cylinders 104. The dish-shaped areas or recesses 252 form valve seats for the respective inlet check valves 194. As shown, for example, in FIG. 7, the perimetrical recess 156, which extends around the elongated recess 154 defined in the front side 140 of the front plate 102 of the pump body 100, also extends around or borders each of the inlet openings 142. Thus, the inlet openings 142 may be sealed by the same sealing element, such as an O-ring, gasket, or weld, disposed about the elongated recess 154, to form a fluid sealing border around the respective dish-shaped recessed areas 252. The sealing element (e.g., O-ring, gasket, or weld) forms a fluid sealing border around the outlet manifold channel 244 and the respective dish-shaped recessed areas 252 when the manifold plate 230 is joined to the front plate 102 of the pump body 100 to form the pump manifold

80. As noted previously, a welded joint, a laser or ultrasonic weld, is preferred in the location of the perimetrical recess **156** in the accompanying figures.

[00144] As described previously, the inlet check valves 194 are held in place in the opposing inlet openings 142 by the respective inlet check valve support structure 144 provided on the front plate 102 of the pump body 100. One or more receiving slots 254 may further be provided in the rear side 234 of the manifold plate 230 and located at spaced circumferential locations around the dish-shaped recesses 252. The one or more receiving slots 254 are adapted to receive corresponding tabs 256 extending from the radial prongs 148 of the inlet check valve support structures 144 provided on the opposing front plate 102 of the pump body 100, thereby securing the inlet check valves 194 opposite the dish-shaped recesses 252 formed in the rear or proximal side 234 of the manifold plate 230. A further purpose of the tabs 256 is to maintain the inlet check valves 194 centered relative to the inlet openings 142. Generally, it is desirable to provide some clearance between the disc edge of the inlet check valves 194 and the wall of the inlet openings 142 to permit fluid to flow past the inlet check valves 194 when opened. The three small tabs 256 keep the inlet check valves 194 centered during operation while leaving most of their circumference free from contact with the wall of the inlet openings 142.

The front side 232 of the manifold plate 230 comprises an outer circumferential [00145] flange or channel 258 which forms a border around the front side 232 of the manifold plate 230, and a series of stiffening ribs 260. The outer flange 258 and stiffening ribs 260 stiffen or provide rigidity to the pump manifold 80 without increasing the thickness of the molded polymeric material forming the pump body 100 and the manifold plate 230. Additionally, the outer flange 258 and the stiffening ribs 260 transfer the clamping force that is applied by the drive and actuating system 400 to the welded joints that are subjected to high stress, as described herein. Moreover, the outer flange 258 and stiffening ribs 260 may also be used for orienting and positioning the pump 10 in association with the drive and actuating system 400 used to operate the pump 10 so that the drive and actuating system 400 may operate the respective drive pistons 50 to capture and independently operate the respective plungers 200 disposed within the pump cylinders 104. The stiffening ribs 260 may be located on the face of the front side 232 of the manifold plate 230, or be formed as part of the outer flange 258 on the front side 232 of the manifold plate 230. A pair of positioning or stiffening tabs 261 may be provided on each of the respective channel members 238 defining the inlet manifold channels 236, and disposed generally between the two (2) circular sets of inlet openings 242 in inlet manifold channels 236. The stiffening tabs 261 help to prevent deflection of the ends

of the pump cylinders **104** when they are subjected to internal fluid pressure, for example, on the order of at least 400 psi and, often, at least 500 psi and greater. Manifold caps **262** are provided for each of the right and left inlet manifold channels **236** and are secured to the respective channel members **238** defining the inlet manifold channels **236** via an ultrasonic or laser welding process and like joining techniques.

The manifold plate 230 is joined to the front side 140 of the front plate 102 of the pump body 100 via a laser welding process and like joining process. This laser welding process secures the manifold plate 230 to the front plate 102 of the pump body 100 and forms a hermetic seal around the fluid paths defined between the manifold plate 230 and the front plate 102. As a result of this laser welding process, the respective sets of inlet openings 242 in the manifold plate 230 are placed in correspondence with the respective inlet openings 142 in the front plate 102 of the pump body 100 to provide fluid communication (across the separating inlet check valves 194) between the right and left inlet manifold channels 236 and the two (2) right and the two (2) left pump cylinders 104, respectively. Further, the laser welding process secures the inlet check valves 194 in association with the respective dishshaped recesses 252 which form the valve seats for the inlet check valves 194. The inlet check valves 194 are held in place in the inlet openings 142 by the respective inlet check valve support structures 144, as mentioned previously. Additionally, the laser welding process secures the engaging tabs 256 associated with the radial prongs 148 of the inlet check valve support structures 144 in their corresponding receiving slots 254 in the rear proximal side 234 of the manifold plate 230, thereby further securing and aligning the inlet check valves 194 in the dish-shaped recesses 252 forming the valve seats for the inlet check valves 194. Moreover, the laser welding process places the outlet manifold channel 244 in fluid communication (across the separating outlet check valves 196) with the respective sets of outlet openings 162 and top openings 160 in the front plate 102 to permit fluid to exit the pump chambers 106 of the respective pump cylinders 104 and enter the outlet manifold channel 244. The outlet check valves 196 are similarly secured and aligned in the outlet check valve receiving recesses 246 in the outlet manifold channel 244 and opposite the plurality of recessed areas 158 defined in the elongated recess 154 on the front side 140 of the front plate 100 during the laser welding process. The plurality of recessed areas 158 forms the valve seats for the respective outlet check valves 196 in a similar manner to the way the dishshaped recesses 252 form valve seats for the inlet check valves 194. Furthermore, the laser welding process provides a weld joint in the perimetrical recess 156, described previously, which forms a fluid sealing border around the outlet manifold channel 244 and the respective

dish-shaped recessed areas **252** when the manifold plate **230** is joined to the front plate **102** of the pump body **100**.

Referring further to FIGS. 20-21, in operation, when the pressure in the inlet [00147] manifold channels 236 is greater than the pressure within the associated pump cylinders 104, the inlet check valves 194 deform to allow fluid flow, designated by arrows F_1 , into the pump chamber 106 of the associated pump cylinders 104. When the pressure within the pump cylinders 104 is greater than the pressure within the associated inlet manifold channels 236, the inlet check valves 194 are pressed against the dish-shaped recesses 252 formed in the rear or proximal side 234 of the manifold plate 230, and prevent fluid flow out of the pump cylinders 104 into the corresponding inlet manifold channel 236. Similarly, when pressure within the pump cylinders 104 is greater than pressure in the outlet manifold channel 244, the outlet check valves 196 associated with the pump cylinders 104 deform to allow fluid flow, as designated by arrows F₂, from the pump cylinder 104. When the pressure in the outlet manifold channel 244 is greater, the outlet check valves 196 associated with the pump cylinders 104 are pressed into the respective recessed areas 158 defined in the elongated recess 154 on the front side 140 of the front plate 102 to seal the respective sets of outlet openings 162 and top openings 160 in the front plate 102 leading to the pump chambers 106 of the pump cylinders 104 and prevent fluid flow from the outlet manifold channel 244 into the pump cylinders **104**.

[00148] Referring additionally to FIGS. 22-26, the manifold plate 230 further comprises an outlet selector valve cylinder 264 extending upward from a top portion of the manifold plate 230 and, in particular, upward from the outer flange 258 which forms a border around the front side 232 of the manifold plate 230. The outlet selector valve cylinder 264 defines a valve bore 266 to accept the body of the outlet selector valve 280 therein. The valve bore 266 and a connecting passage 268 thereto are desirably located above the outlet manifold channel 244, permitting any air that is initially trapped in the outlet manifold channel 244 to rise up into the connecting passage 268 and valve bore 266 during the fluid priming process.

[00149] The outlet selector valve 280 controls fluid delivery or output from the pump 10. The valve bore 266 is in fluid communication with the outlet manifold channel 244 via the connecting passage 268. The outlet selector valve cylinder 264 further defines a pair of outlet ports 270, 272, including a patient outlet port 270 that accepts a swabable valve 274 and a waste outlet port 272. The swabable valve 274 may be secured within the patient outlet port 270 via medical grade adhesive, solvent bonding, laser and ultrasonic welding, and like joining techniques. As an alternative, the patient port 270 may be overmolded around the

stem of the swabable valve 274, which eliminates the need for adhesive, solvents, or welding. The swabable valve 274 is generally used to connect the patient supply set 40 to the patient outlet port 270. Because the valve is swabable, multiple connections may be made without compromising the connection. A self-sealing silicone stem (not shown) in the swabable valve 274 also prevents fluid drips when the patient supply set 40 is removed.

The outlet selector valve 280 comprises a unitary outlet selector valve body 282 with an actuator interface head 284 and a depending valve stem 286 that terminates in a rounded or tapered bottom edge or end 288. Suitable material choices for the outlet selector valve body 282 include, but are not limited to: polyethylene (plain and fiber reinforced), polypropylene, nylon (including fiber reinforced), Ultem® PEI (polyetherimide), polycarbonate (plain and with silicone or siloxane), and like materials. The valve stem 286 defines a 90° flow passage 290 which tapers smoothly to the bottom edge or end 288 of the valve stem 286. The "bell" shape of the flow passage 290 which tapers to the rounded bottom end 288 of the valve stem 286 minimizes the potential for air bubbles to become trapped below the valve stem 286. The flow passage terminates 290 at one side of the valve stem 286 to define an outlet port 291 for fluid communication with the patient outlet port 270 and the waste outlet port 272. The actuator interface head 284 of the outlet selector valve body 282 is adapted to interface with a valve actuator, described herein, associated with the drive and actuating system 400 which operates the pump 10. The valve actuator controls operation of the outlet selector valve 280 to place the valve stem 286 in orientations at least to: (1) place the flow passage 290 in fluid communication with the patient outlet port 270 and, thus, in fluid communication with the connecting passage 268 leading to the outlet manifold channel 244; (2) place the flow passage 290 in fluid communication with the waste outlet port 272 and, thus, in fluid communication with the connecting passage 268 leading to the outlet manifold channel 244; and (3) place the flow passage 290 in a shut-off position or "off" position where the flow passage 290 is not aligned with either the patient outlet port 270 or the waste outlet port 272, thereby preventing fluid flow from the outlet manifold channel 244 to either outlet port 270, 272.

[00151] The actuator interface head 284 is generally T-shaped and comprises, for example, two (2) outwardly extending tabs 292 and a recessed area 294 for engagement with the valve actuator associated with the drive and actuating system 400, detailed hereinw. The T-shape of the actuator interface head 284 allows the outlet selector valve body 282 to slide into engagement with the valve actuator and also "keys" the outlet selector valve body 282 so that it may be engaged by the valve actuator in only one particular orientation. This interface

between the actuator interface head **284** and the valve actuator of the drive and actuating system **400** also prevents the outlet selector valve body **282** from being ejected upward from the outlet selector valve cylinder **264** on the manifold plate **230** under high operating pressure.

[00152] Additionally, the outlet selector valve **280** comprises a rear or proximal pressure sensing port 296 defined in the outlet selector valve cylinder 264 supporting the outlet selector valve body 282 that supports a pressure sensing diaphragm 298, which interfaces with the drive and actuating system 400 so that fluid pressure in the valve bore 266 may be measured. The pressure sensing diaphragm 298 is a thin polyurethane (and like polymeric materials) diaphragm that is used to measure the fluid pressure in the outlet manifold channel 244. The pressure sensing diaphragm 298 is desirably overmolded into the pressure sensing port 296 and seals the port 296 while transferring the fluid pressure within the pressure sensing port 296 to its exterior surface. The pressure sensing diaphragm 298 allows the pressure in the outlet manifold channel 244, which is connected to the valve bore 266 via the connecting passage 268, to be measured at any time, not just when injecting fluid into a patient. As one example, during fluid priming or flushing operations, the control system 800 can monitor the pressure in the outlet manifold channel 244 and determine if the waste collection tube set 46 is blocked or kinked. A load cell or like device, provided as part of the drive and actuating system 400, interfaces with the diaphragm 298 to measure the fluid pressure through the diaphragm 298, as described herein in connection with the drive and actuating system 400.

[00153] As noted previously, the waste collection system 44 is connected to the waste outlet port 272 on the outlet selector valve cylinder 264 on the manifold plate 230 and is used to collect and store waste fluids. In particular, the waste collection tube set 46 is connected to the waste outlet port 272 to conduct waste fluids to the waste collection container 48 when the outlet selector valve 280 is actuated to place the flow passage 290 in fluid communication with the waste outlet port 272.

[00154] FIGS. 25A-25Q illustrate additional embodiments of the outlet selector valve body 282, wherein the outlet selector valve body 282 is embodied with different sealing arrangements. In a first such example shown in FIGS. 25A-25C, a lip seal arrangement 1200 is provided which comprising compliant overmolded lips seals formed, for example, of thermoplastic material such as TPU (thermoplastic polyurethane), on the rigid valve stem 286. The compliant seals allow the valve stem 286 to be sealed in the valve bore 266 of the outlet selector valve cylinder 264 on the manifold plate 230. The valve stem 286 may be a

rigid polycarbonate stem having the attached flexible thermoplastic lip seal arrangement 1200. The lip seal arrangement 1200 comprises a lower lip seal 1202 that provides a compliant seal between a lower portion of the valve stem 286 and the valve bore 266 and centers the valve stem 286 within the valve bore 266. Additionally, the lip seal arrangement 1200 comprises an upper lip seal 1204 that prevents ingress of foreign particles into the valve bore **266** and prevents fluid from exiting the valve bore **266** if any of the other lip seals leak. Further, the lip seal arrangement 1200 comprises a port lip seal 1206 that surrounds the outlet port 291 defined by the flow passage 290 on the sidewall of the valve stem 286 and provides a compliant seal between the sidewall of the valve stem 286 and the valve bore 266 of the outlet selector valve cylinder 264 on the manifold plate 230. Moreover, the lip seal arrangement 1200 comprises an isolation seal 1208 that is located on the valve stem 286 at a position approximately 180° opposite from the port lip seal **1206**. The isolation seal **1208** is used to isolate the patient outlet port 270 from the waste outlet port 272 when the valve stem **286** is in the "off" position, wherein each of these ports are isolated from one another and the flow passage 290. The geometry of the lip seals 1202, 1204, 1206 provide a higher level of sealing force when high pressure fluid is in contact with the seals (e.g., the seals are hydraulically energized).

[00155] The flow passage 290 has an inlet at the bottom of the valve stem 286 and is always connected to the outlet manifold channel 244, as described previously The outlet port 291 is located on the sidewall of the valve stem 286 and may be rotated to direct flow to either the patient outlet port 270 or the waste outlet port 272. The shape of the flow passage 290 minimizes the potential for trapping air bubbles, as described previously. Additionally, as the outlet port 291 is at a higher elevation than the inlet to the flow passage 290, there is a natural tendency for air bubbles to rise to the selected outlet port, the patient outlet port 270 or the waste outlet port 272, and be ejected typically from the outlet selector valve 280 via the waste outlet port 272.

[00156] The diameter of the lip seals 1202, 1204, 1206 is slightly larger than the diameter of the valve bore 266 so that when the valve stem 286 is assembled into the valve bore 266, the lip seals 1202, 1204, 1206 are slightly compressed against the wall of the valve bore 266. At low fluid pressures, the initial compression from the assembly process is sufficient to seal against low fluid pressures and, because the seals are compliant and easily deformed, the sealing force (and frictional torque) between the valve stem 286 and the valve bore 266 of the outlet selector valve cylinder 264 is low. At high fluid pressures, the lip seals 1202, 1204, 1206 become "hydraulically energized." The hydraulic pressure of the fluid against the lip

seals 1202, 1204, 1206 creates an additional sealing force. This additional force presses the lip seals 1202, 1204, 1206 more firmly against the outlet selector valve cylinder 264 as the pressure increases, and higher pressures result in greater sealing forces without requiring a large degree of initial compression.

[00157] When the valve stem 286 is positioned so that the flow passage 290 is in fluid connection with the patient outlet port 270, the lower lip seal 1202 prevents high pressure fluid from entering the annular space around the valve stem 286. The port lip seal 1206 directs fluid from the center of the flow passage 290 to the patient outlet port 270 and prevents high pressure fluid from entering the annular space around the valve stem 286. Because there is no port in the outlet selector valve cylinder 264 that is directly across from the patient outlet port 270, the isolation seal 1208 is not required when the valve stem 286 is in this position. As fluid is ejected through the outlet port 291, there is a hydraulic reaction force that tends to push the valve stem 286 away from the patient outlet port 270. Rigid support pads 1210 may be provided on the side of the valve stem 286 to resist this reaction force and prevent the lower lip seal 1202 from being deformed excessively. Under normal operating conditions, the upper lip seal 1204 is used to keep the valve stem 286 centered in the valve bore 266, and prevents fluid egress if one of the other lip seals leaks.

[00158] When the valve stem 286 is positioned so that the flow passage 290 is in fluid connection with the waste outlet port 272, the lower lip seal 1202 prevents low pressure fluid from entering the annular space around the valve stem 286. The port lip seal 1206 directs fluid from the center of the flow passage 290 to the waste outlet port 272 and prevents low pressure fluid from entering the annular space around the valve stem 286. Because there is no port in the outlet selector valve cylinder 264 that is directly across from the waste outlet port 272, the isolation seal 1208 is not required when the valve stem 286 is in this position. The patient outlet port 270 is connected to the annular space around the valve stem 286 and, because this annular space is not connected to any other port at this time, the patient outlet port 270 remains isolated from all other ports. Under normal operating conditions, the upper lip seal 1204 is used to keep the valve stem 286 centered in the valve bore 266, and prevents fluid egress if one of the other lip seals leaks.

[00159] In a second sealing example shown in FIG. 25D, the valve stem 286 is formed with a thin cylindrical wall 1212 and an elastomeric core 1214 is disposed in the thin-walled cylindrical valve stem 286. The open center of the valve stem 286 is filled with a compliant elastomeric core 1214 made from materials such TPU (thermoplastic urethane) or silicone rubber, and defines the flow passage 290 to provide a defined fluid pathway through the

valve stem 286. The thin cylindrical sidewall 1212 defines an aperture 1216 connected to the outlet port 291 of the flow passage 290. The upper portion of the valve body 282 maintains the features described previously for interfacing with the drive and actuating system 400. The thin cylindrical wall 1212 of the valve stem 286 and forming the lower portion of the valve body 282 may be easily deformed to allow the outside diameter of the valve stem 286 to conform to and seal against the valve bore 266 of the outlet selector valve cylinder 264. The elastomeric core 1214 defines the flow passage 290, which serves to direct fluid from the inlet thereto to the outlet port 291 connected to the aperture 1216 in the valve stem 286, and the flow passage 290 maintains the features described previously for minimizing the potential for trapped air and stagnant regions in the flow path. The elastomeric core 1214 is generally soft and compliant enough that it does not significantly stiffen the cylindrical wall or walls 1212 of the valve stem 286. When the valve stem 286 is subjected to internal pressure, the cylindrical sidewall 1212 of the valve stem 286 expands outward to increase the sealing force between the outer diameter of the valve stem 286 and the valve bore 266.

In a third sealing example shown in FIGS. 25E-25G, a sealing arrangement 1220 similar to sealing arrangement 1200 described previously is provided but now comprises a plurality of o-ring seals on the valve stem 286, which is a rigid polycarbonate stem and has the same general structure as described previously in connection with FIGS. 24A-24B and FIGS. 25A-25C. In one embodiment of the sealing arrangement 1220, four (4) o-ring seals 1222-1228 are installed in grooves molded in the valve stem 286. A first o-ring seal 1222 provides a compliant seal between the lower portion of the valve stem 286 and the valve bore 266 and centers the valve stem 286 within the valve bore 266. A second o-ring seal 1224 prevents the ingress of foreign particles into the valve bore 266 and prevents fluid from exiting the valve bore 266 if any of the other seals leak. A third o-ring seal 1226 surrounds the outlet port 291 in the sidewall of the valve stem 286 and provides a compliant seal between the valve stem 286 and valve bore 266 of the outlet selector valve cylinder 264. A fourth isolation o-ring seal 1228 is located on the valve stem approximately 180° opposite from the third o-ring seal 1226 surrounding the outlet port 291. The isolation o-ring seal 1228 is used to isolate the patient outlet port 270 from the waste outlet port 272 when the valve stem 286 is in the "off" position. The o-ring seals 1222-1228 may be made of any type of suitable elastomeric material including polyurethane, silicone or EPDM.

[00161] In a hybrid embodiment shown in FIGS. 25H-25I, the valve stem 286, as shown in FIG. 25D having a thin cylindrical wall 1212 and an elastomeric core 1214 disposed in the thin-walled cylindrical valve stem 286, is combined with a sealing o-ring 1230 disposed in a

groove in or seated against a ledge 1232 defined by the upper portion of the valve stem 286. The o-ring 1230 may be made of silicone rubber, polyurethane, EPDM or other suitable elastomer. Any fluid that may leak between the valve stem 286 and the outlet selector valve cylinder 264 is prevented from leaking outside of the outlet selector valve cylinder 264 by the upper o-ring 1230 at the top of the valve stem 286.

[00162] In another sealing arrangement 1234 as shown in FIGS. 25J-25L, the valve stem 286 is segmented to define a plurality of finger elements 1236 with spaces 1238 in-between, and the valve stem 286 is enclosed by a cooperating sleeve element 1240. Each finger element 1236 acts like a cantilevered leaf spring that is biased to expand outward against the wall of the valve bore 266. The finger elements 1236 may be molded in a cylindrical configuration, as shown, or may be molded in a conical formation such that the finger elements 1236 compress inward to initially install the valve stem 286 into the valve bore 266. In either configuration, the finger elements 1236 provide a radial outward force against the valve bore 266 to improve sealing.

[00163] The sleeve element 1240 serves as the sealing surface against the wall of the valve bore 266 and may be made of TPU and other suitable elastomeric materials. The sleeve element 1240 comprises internal, axially-extending radial ridges 1242 that are trapped in the spaces 1238 in-between the finger elements 1236, forcing the finger elements apart 1236 and radially-outward. The sleeve element 1240 further defines the upper end of the flow passage 290 and corresponding apertures 1246, 1248 are defined in the valve stem 286 and the sleeve element 1240, respectively, to define the outlet port 291 of the flow passage 290. In use with low fluid pressures, the spring action of the finger elements 1236 presses the sleeve element 1240 radially outward until it is sealed against the wall of the valve bore 266. The radial ridges 1242 that are trapped in the spaces 1238 in-between the finger elements 1236 may also help to force the finger elements 1236 circumferentially apart, increasing the sealing force. In use with high fluid pressures, fluid pressure inside of the flow passage 290 in the valve stem 286 also helps to generate a radial-outward force on the finger elements 1236 and the sleeve element 1240, increasing the sealing force against the wall of the valve bore 266.

[00164] In another sealing arrangement 1250 as shown in FIGS. 25M-25N, the valve body 282 is of composite form, namely having an upper portion 1252 formed of a stiff polycarbonate material or like material, and a compliant lower portion 1254 formed of TPU or other suitable elastomeric materials. The lower portion 1254 generally forms the valve stem 286 while the upper portion 1252 defines the features described previously for interfacing with the drive and actuating system 400. The lower portion 1254 generally

forming the valve stem **286** has integral upper and lower sealing beads **1256**, **1258** to seal against the wall of the valve bore **266** and another sealing bead **1260** to form a seal about the outlet port **291** of the flow passage **290** to create sufficient sealing force around this port. The material used for the lower portion **1254** generally forming the valve stem **286** may have a higher durometer (and higher stiffness) than the material used for the various fluid seals in the preceding sealing arrangements described in connection with **FIGS. 25A-25L**.

In yet another sealing arrangement 1270 as shown in FIGS. 25O-25Q, a sleeve or liner 1272 formed of compliant sealing material is seated within the valve bore 266 of the outlet selector valve cylinder 264 instead of on the valve stem 286. The valve body 282 has the same general configuration as described previously in connection with FIGS. 24A-24B, with the addition of an upper ridge or ledge or sealing bead 1274 formed below the actuator interface head 284 and an exterior raised bead 1276 around the outlet port 291 of the flow passage 290 in the valve stem 286 to ensure suitable sealing characteristics in the valve bore 266. The valve body 282 may be made of a rigid material such as polycarbonate. The elastomeric sleeve or liner 1272 may be made of TPU or a similar elastomer. The liner 1272 defines an upper recessed area 1278 to receive the ridge or ledge and/or sealing bead 1274 provided on the valve stem 286, and defines respective side apertures 1280 to provide fluid communication with the outlet port 291 of the flow passage 290 in the valve stem 286, and the patient outlet port 270 and the waste outlet port 272. The liner 1272 may include one or more axial recessed areas 1282 to prevent contact with the exterior raised bead 1276 around the outlet port 291 of the flow passage 290, and this axial recessed area 1282 is a suitable location to orient the raised bead 1276 during shipment or storage of the pump device 10. By placing the raised bead 1276 in the recessed area 1282 during shipping and storage, the liner 1272 is less likely to experience compression set or creep which could cause a reduction in sealing characteristics. It may also be desirable to integrate the pressure sensing diaphragm **298** as part of the liner **1272** to consolidate components.

[00166] Referring further to FIGS. 27-29, as noted in the foregoing, an inlet selector valve 300 is provided in each of the inlet selector valve cylinders 114. Each inlet selector valve cylinder 114 defines a cylindrical chamber 116 that accepts the inlet selector valve 300 which is rotationally operable within the inlet selector valve cylinder 114. The drive and actuating system 400 which operates the pump 10 also desirably includes separate valve actuators that operate the respective inlet selector valves 300. The respective inlet selector valves 300 each comprise an inlet selector valve body 302 with an actuator interface head 304 and an elongated and hollow valve stem 306 that terminates in a distal edge or end 308 which abuts

(or is disposed in proximity to) the front plate 102 and extends about the front or distal end opening 118 formed in the front plate 102. The valve stem 306 defines an axial bore or passage 310. The actuator interface head 304 of the inlet selector valve body 302 is adapted to interface with an inlet selector valve actuator, described herein, associated with the drive and actuating system 400. The actuator interface head 304 may be generally round or circular in shape and comprises a proximally extending tab 312, or a plurality of such tabs 312, and an interface engagement member 314 formed internally within the actuator interface head 304. The proximally extending tab 312 and internal engagement member 314 form interfacing features for engagement with the inlet selector valve actuator associated with the drive and actuating system 400. For safety purposes, it is desirable for the valve stem 306 to be engaged to the drive and actuating system 400 in one particular angular orientation. If the valve stem 306 can be installed in more than one angular orientation, it could be possible to deliver the wrong type of fluid, as described further herein.

The valve stem 306 defines a series of radial inlet openings or ports 320 that connect to the central or axial passage 310. The radial inlet openings or ports 320 are located at different angular locations around the valve stem 306 and at different axial locations along the valve stem 306. The radial inlet openings or ports 320 include a first inlet port 322 for placing the first inlet port 122 on the receiving inlet selector valve cylinder 114 in fluid communication with the axial passage 310 in the valve stem 306, a second inlet port 324 for placing the second inlet port 124 on the receiving inlet selector valve cylinder 114 in fluid communication with the axial passage 310 in the valve stem 306, and third and fourth inlet ports 326, 328 positioned to allow fluid communication between either of the saline channels 132, 134 of the saline manifold 130 and the axial passage 310 in the valve stem 306. The respective inlet ports 322, 324, 326, 328 are defined at different angular locations around the valve stem 306 and are positioned at spaced axial locations along the valve stem 306 so that, at most, only one of these inlet ports 322-328 permits fluid communication with the axial passage 310 in the valve stem 306 at any given time, and thereby permit fluid flow into the valve stem 306 from the first inlet port 122, second inlet ports 124, or one of the saline channels 132, 134. In particular, the respective inlet ports 322-328 are defined at different angular locations around the valve stem 306 and spaced axial locations along the valve stem 306 so that only one of the first and second inlet ports 122, 124 and the saline channels 132, 134 of the saline manifold 130 is in fluid communication with the axial bore or passage 310 in the valve stem 306 at any given time. Accordingly, if the first inlet port 322 is in fluid communication with the first inlet port 122, the second inlet port 124 is blocked by the valve

stem 306 to fluid flow, as are both of the saline channels 132, 134 of the saline manifold 130. Similarly, if the second inlet port 324 is in fluid communication with the second inlet port 124, the first inlet port 122 is blocked by the valve stem 306 to fluid flow, as are both of the saline channels 132, 134 of the saline manifold 130. If the third inlet port 326 is aligned with the first or forward saline channel 132, the first and second inlet ports 122, 124 are blocked to fluid flow by the valve stem 306, as is the second or rearmost saline channel 134. Further, if the fourth inlet ports 122, 124 are blocked to fluid flow by the valve stem 306, as is the first and second inlet ports 122, 124 are blocked to fluid flow by the valve stem 306, as is the first or forward saline channel 132.

In the depicted arrangement, the inlet ports 322-328 are axially spaced along the valve stem 306, with the first inlet port 322 located near the distal end 308 of the valve stem 306 and the last or fourth inlet port 328 located near the actuator interface head 304. As explained previously, the foregoing axial order of the ports 122-126 and corresponding ports 322-328 is desirable for air management issues. In particular, in the pump 10 in the accompanying figures, the "left" saline source S1 is connected to the left saline port 126 so that the rearmost saline channel 134 is filled first with saline for priming purposes. The rearmost or fourth inlet port 334 in the valve stem 306 is located in the rearmost position to establish fluid communication with the rearmost saline channel 134 to allow the entire inlet selector valve 300 to be primed with saline from the far rear or proximal end. If this "saline" port was located in any other "forward" position, it would not be possible to remove all of the air from the length of the inlet selector valve 300 as air would be trapped behind this position. It is noted that the distance from the saline inlet port 328 and the proximal or rear end of axial passage 310 adjacent the actuator interface head 304 is minimized as much as possible to limit the potential for air bubbles to be trapped behind this inlet port 328 and the end of the axial passage 310.

[00169] Referring specifically to FIGS. 28C-28D, the inlet selector valve 300 may be provided with a sealing arrangement 1300 on the valve stem 306. The sealing arrangement 1300 uses a series of elastomeric seals, which are similar to o-rings, to seal the valve stem 306 in the inlet selector valve cylinder 114. Each of the four inlet ports 322-328 is sealed in two (2) ways according the illustrated embodiment. First, a circular sealing bead 1302 is provided around each of the inlet ports 322-328 in the valve stem 306, and this seal prevents any fluid that may be in the central or axial passage 310 of the valve stem 306 from moving into the space between the valve stem 306 and the inlet selector valve cylinder 114. Secondly, two (2) circumferential sealing rings 1304, 1306 are axially located on either side of each

inlet port 322-328, and are used to isolate the inlet ports 322-328 in the inlet selector valve cylinder 114. These circumferential seal rings 1304, 1306 prevent fluids connected to the first inlet port 122, second inlet port 124, or one of the saline channels 132, 134 from mixing with one another in the inlet selector valve cylinder 114. Each of the foregoing seals 1302, 1304, 1306 is made of TPU (thermoplastic polyurethane) or like elastomers and is attached to the rigid valve stem 306 during an overmolding process. The valve stem 306 may be made of polycarbonate and like materials. Each seal 1302, 1304, 1306 has a "D-shaped" cross-section which seals against the inlet selector valve cylinder 114.

[00170] Referring to FIGS. 28E-28F, the inlet selector valve 300 may be provided with an alternative sealing arrangement 1310 on the valve stem 306. In this embodiment, a soft (TPU - thermoplastic polyurethane, or like material) sleeve 1312 is overmolded onto the rigid valve stem 306, which may be polycarbonate to provide rigidity and torsional stiffness to the valve stem 306. The overmolded sleeve 1312 provides a compliant surface to allow the valve stem 306 to seal against the against the inlet selector valve cylinder 114. The compliant surface allows the valve stem 306 to fully seal against the interior wall of the inlet selector valve cylinder 114 even if surface imperfections are present in either component.

With the foregoing radial and axial locations for the inlet ports 322-328, the inlet selector valve actuators, described herein, of the drive and actuating system 400 control operation of the right and left inlet selector valves 300 to place the valve stem 306 in an orientation to: (1) connect the first inlet port 322 with the first inlet port 122 to provide fluid communication between a first source of therapeutic or diagnostic (e.g., pharmaceutical) fluid A1, B1 contained in a connected fluid source container 30 and the corresponding inlet manifold channel 236, while the second inlet port 124 and both of the saline channels 132, 134 of the saline manifold 130 are blocked to fluid flow by the valve stem 306; (2) connect the second inlet port 324 with the second inlet port 124 to provide fluid communication between a second source of therapeutic or diagnostic (e.g., pharmaceutical) fluid A2, B2 contained in a connected fluid source container 30 and the corresponding inlet manifold channel 236, while the first inlet port 122 and both of the saline channels 132, 134 of the saline manifold 130 are blocked to fluid flow by the valve stem 306; (3) connect the third inlet port 326 with the first or forward saline channel 132 of the saline manifold 130 to connect the third inlet port 326 with the first or forward saline channel 132 of the saline manifold 130 via saline port 332 (FIG. 5B) to provide fluid communication between a second source of saline S2 contained in a connected fluid source container 30 and the corresponding inlet manifold channel 236, while the first and second inlet ports 122, 124 and

the second or rear saline channel 134 of the saline manifold 130 are blocked to fluid flow by the valve stem 306; (4) connect the fourth inlet port 328 with the second or rearmost saline channel 134 of the saline manifold 130 via saline port 334 (FIG. 5B) to provide fluid communication between a first source of saline S1 contained in a connected fluid source container 30 and the corresponding inlet manifold channel 236, while the first and second inlet ports 122, 124 and the first or forward saline channel 132 of the saline manifold 130 are blocked to fluid flow by the valve stem 306; and (5) an "OFF" position wherein the valve stem 306 is in a position to block each of the first and second inlet ports 122, 124 and the first and second saline channels 132, 134, thereby preventing fluid flow from the various external fluid sources contained in the fluid source containers 30 to the corresponding inlet manifold channel 236. Thus, at least a total of five (5) different operational states are present for each of these inlet selector valves 300 in the embodiment of the pump 10 found in the accompanying figures. However, this embodiment should not be considered limiting as additional inlet ports (not shown) may be provided on the respective inlet selector valve cylinders 114, with corresponding inlet ports (not shown) being provided in the valve stem 306 of the respective inlet selector valves 300 to accommodate additional connected fluid sources as desired.

Referring specifically to FIGS. 5A and 5B, it will be understood that the saline manifold 130 is formed to extend across the pump cylinders 104 and has opposing ends that connect to the respective inlet selector valve cylinders 114. With this construction, the saline channels 132, 134 extend the length between the two (2) outboard inlet selector valve cylinders 114. Saline ports 332, 334 are defined in the bottom of each of the inlet selector valve cylinders 114 to connect the inlet selector valve cylinders 114 to the saline channels 132, 134. The first or forward saline ports 332 connect the inlet selector valve cylinders 114 to the first or forward saline channel 132 and the second or rear saline ports 334 connect the inlet selector valve cylinders 114 to the second or rear saline channel 134. Accordingly, when the valve stem 306 of the actuated inlet selector valve 300 is rotated to connect the third inlet or "saline" port 326 with the first or forward saline channel 132 of the saline manifold 130, the third inlet "saline" port 326 is actually aligned with the first or forward saline port 332 in the inlet selector valve cylinder 114. Additionally, when the valve stem 306 of the actuated inlet selector valve 300 is rotated to connect the fourth inlet "saline" port 328 with the second or rear saline channel 134 of the saline manifold 130, the fourth inlet or "saline" port 328 is actually aligned with the second or rear saline port 334 in the inlet selector valve cylinder 114.

In the exemplary configuration of the pump 10 depicted in the accompanying [00173] figures, the left side inlet ports 122, 124 may be connected, respectively, to two (2) different sources of therapeutic or diagnostic (e.g., pharmaceutical) fluids, A1, A2, to be received in the two (2) left pump cylinders 104, and the left side saline port 126 may be connected to a first source of saline, designated as "S1". Fluid "A1" provided in one of the fluid source containers 30 may be connected to first inlet port 122 and fluid "A2" provided in one of the fluid source containers 30 may be connected to the second inlet port 124, or vice versa, on the left side 18 of the pump 10. Likewise, the right side inlet ports 122, 124 may be connected, respectively, to two (2) different sources of therapeutic or diagnostic (e.g., pharmaceutical) fluid, **B1**, **B2** to be received in the two (2) right pump cylinders **104**, and the right side saline port 126 may be connected to the second source of saline, designated as "S2". The two (2)channel saline manifold 130 permits saline from either saline source S1, S2 to be pulled into either of the inlet selector valves 300 during operation of the pump 10. Fluid "B1" provided in one of the fluid source containers 30 may be connected to first inlet port 122 and fluid "B2" provided in one of the fluid source containers 30 may be connected to the second inlet port 124, or vice versa, on the right side 16 of the pump 10. Further, fluids A1, A2 may be connected to the right side inlet ports 122, 124 in any desired pairing, and the fluids B1, B2 may be connected to the left side inlet ports 122, 124 in any desired pairing as an alternative configuration for the pump 10. Accordingly, for exemplary purposes only in this disclosure, fluid flow of the fluids A1, A2 contained in the fluid source containers 30 is controlled by the left side inlet selector valve 300 and fluid flow of the fluids B1, B2 contained in the fluid source containers 30 is controlled by the right side inlet selector valve 300. As noted previously, the respective inlet selector valves 300 may draw saline from either of the saline channels 132, 134 of the saline manifold 130. Hence, the respective inlet selector valves 300 may draw from either saline source S1, S2. Accordingly, each "half" of the pump 10 has a single inlet selector valve 300 that allows selection from several fluid sources that are to be fed into the two (2) associated pump cylinders 104. Thus, control of fluids to the two (2) left side pump cylinders 104 is provided by the left side inlet selector valve 300 and control of fluids to the two (2) right side pump cylinders 104 is provided by the right side inlet selector valve **300**.

[00174] The initial angular orientation of the valve stem 306 of the inlet selector valves 300 may be preset by the manufacturer and this orientation may be encoded into the pump indicator plate 170 and/or into identifying indicia 172 on the pump body 100, described previously. The control system 800 can thereby determine the initial or preset angular

orientation of the valve stem **306** and operate the drive and actuating system **400** accordingly. If the angular orientation of the valve stem **306** is not needed for control by the control system **800** (such as if a read-write RFID tag is used for the identifying indicia **172**) the valve stem **306** of the inlet selector valves **300** may have any suitable initial angular orientation such as the "OFF" position outlined previously. Once associated with the drive and actuating system **400**, the respective plungers **200** may be driven forward into the pumping zone **164** of the pump chambers **106** until the distal end of the plunger **200** contacts the distal end wall **110** of the pump cylinder **104**. Priming of the various fluid pathways in the pump **10** may be then be conducted.

[00175] The storage/isolation zone 166 has a larger diameter than the primary working/pumping zone 164 in each of the pump cylinders 104 to allow the forward or distal end lip seal 218 to reside in an uncompressed state within the large diameter storage/isolation zone 166 during storage. If this seal 218 was stored in the working/pumping zone 164, there is the possibility that the seal 218, over time, could "creep" or "relax" or take a compression set to the point that it would no longer be adequately squeezed/compressed during use, preventing it from sealing appropriately.

Referring further to FIGS. 30-36, general operation of one of the "primed" pump [00176] cylinders 104 in the pump 10 will now be provided with reference primarily to the right outboard pump cylinder 104 of the pump body 100 as shown in FIGS. 32-36. Initially, as shown by the horizontal cross-sectional view of the pump 10 shown in FIG. 30, the respective plungers 200 are located in the isolation zone 166 in the pump chamber 106 of the respective pump cylinders 104, and the inlet selector valves 300 are in the "OFF" position. Assuming priming of the fluid pathways in the pump 10 has been completed, the right side selector valve 300 may be actuated to, for example, place the valve stem 306 in an angular orientation in the inlet selector valve cylinder 114 to permit fluid communication between the first inlet port 322 in the valve stem 306 and the first inlet port 122 on the right inlet selector valve cylinder 114, as shown in FIG. 32. Retraction of the plunger 200 in the pump chamber 106 of the right outboard pump cylinder 104 results in fluid B1 in the connected fluid source container 30 being drawn through the axial passage 310 in the valve stem 306 and into the right side inlet manifold channel 236 to act upon the underlying inlet check valve 194 and open the inlet check valve 194 (see also the previous discussion of FIG. 20). The fluid flow acts upon the inlet check valve 194 supported by the inlet check valve support structure 144 in the inlet opening 142 and opens the inlet check valve 194 so that fluid B1 may pass through the inlet opening 142 and enter the pump chamber 106 of the pump cylinder 104.

The inlet check valve 194 regulates the fluid flow into the pump chamber 106 of the pump cylinder 104. The fluid flow of fluid B1 is identified by arrow A_1 in FIG. 32.

[00177] Next, if desired, a second therapeutic or diagnostic (e.g., pharmaceutical) fluid may be drawn into the pump chamber 106 of the right outboard pump cylinder 104 to be mixed with the fluid **B1** present in the pump chamber **106**. If so, the right side selector valve **300** may be actuated to place the valve stem **306** in an angular orientation in the inlet selector valve cylinder 114 to permit fluid communication between the second inlet port 324 in the valve stem 306 and the second inlet port 124 on the inlet selector valve cylinder 114, as shown in FIG. 33. Additional retraction of the plunger 200 in the pump chamber 106 of the right outboard pump cylinder 104 results in fluid B2 in the connected fluid source container 30 being drawn through the axial passage 310 in the valve stem 306 and into the right side inlet manifold channel 236 to act upon the underlying inlet check valve 194 and open the inlet check valve 194 (see also the previous discussion of FIG. 20). The fluid flow acts upon the inlet check valve 194 supported by the inlet check valve support structure 144 in the inlet opening 142 and opens the inlet check valve 194 so that the fluid B2 may pass through the inlet opening 142 and enter the pump chamber 106 of the pump cylinder 104. The inlet check valve 194 regulates the fluid flow into the pump chamber 106 of the pump cylinder 104. The fluid flow of fluid **B2** is identified by arrow **A2** in **FIG. 33**. In the scenario presented in the foregoing, it is assumed that fluid **B1** is different from fluid **B2**, but these fluids may also be the same medical fluid as well. This example is provided to illustrate mixing of fluids in the respective pump chambers 106 of the pump cylinders 104, if so desired, and with appropriate safety protocols in the control system 800 relating to the mixing of fluids. As an alternative, if the fluids B1, B2 are the same fluid, the fluid delivery system 2 may deliver fluid continuously from the fluid source container 30 holding fluid B1 until this container is exhausted, and the system 2 may then switch to the "backup" fluid source container 30 holding fluid **B2**.

[00178] Further, if desired, saline from the saline sources S1, S2 contained in the connected saline fluid source containers 30 provided on opposite sides of the pump 10 may be drawn into the pump chamber 106 of the right outboard pump cylinder 104 to be mixed with the fluids B1, B2 present in the pump chamber 106. The rights side inlet selector valve 300 may be operated to draw from either saline source S1, S2. In a desirable operational practice, mixing saline S1, S2 with fluids B1 and/or B2 can occur by delivering saline with the two (2) pump cylinders 104 on one side of the pump 10 and delivering the diagnostic or therapeutic (e.g., pharmaceutical) fluids B1, B2 with the two (2) pump cylinders 104 on the

other side of the pump 10. In the present example, if it is desired, for example, to next mix in saline S2, the right side selector valve 300 may be actuated to place the valve stem 306 in an angular orientation to permit fluid communication between the third inlet port 326 in the valve stem 306 and the saline port 332 in the inlet selector valve cylinder 114 which connects to the first or forward saline channel 132 of the saline manifold 130, as shown in FIG. 34. Further retraction of the plunger 200 in the pump chamber 106 of the right outboard pump cylinder 104 results in saline S2 in the connected fluid source container 30 being drawn from the saline channel 132 through the saline port 332 in the inlet selector valve cylinder 114 into the axial passage 310 in the valve stem 306 and into the right side inlet manifold channel 236 to act upon and open the underlying inlet check valve 194 (see also the previous discussion of FIG. 20). The fluid flow acts upon the inlet check valve 194 supported by the inlet check valve support structure 144 in the inlet opening 142 and opens the inlet check valve 194 so that the saline S2 may pass through the inlet opening 142 and enter the pump chamber 106 of the pump cylinder 104. The inlet check valve 194 regulates the fluid flow into the pump chamber 106 of the pump cylinder 104. The fluid flow of saline S2 is identified by arrow A3 in FIG. 34.

[00179] Moreover, if saline S1 is also desired to be mixed into the fluids B1, B2 and saline S2 now present in the pump chamber 106 of the pump cylinder 104, the right side selector valve 300 may be actuated to place the valve stem 306 in an angular orientation to permit fluid communication between the fourth inlet port 328 in the valve stem 306 and the saline port 334 in the inlet selector valve cylinder 114 which connects to the second or rearmost saline channel 134 of the saline manifold 130, as shown in FIGS. 35-36. Further retraction of the plunger 200 in the pump chamber 106 of the right outboard pump cylinder 104 results in saline S1 in the connected fluid source container 30 being drawn from the saline channel 134 through the saline port 334 in the inlet selector valve cylinder 114 into the axial passage 310 in the valve stem 306 and into the right side inlet manifold channel 236 to act upon and open the underlying inlet check valve 194 (see also the previous discussion of FIG. 20). The fluid flow acts upon the inlet check valve 194 supported by the inlet check valve support structure 144 in the inlet opening 142 and opens the inlet check valve 194 so that the saline S1 may pass through the inlet opening 142 and enter the pump chamber 106 of the pump cylinder 104. The inlet check valve 194 regulates the fluid flow into the pump chamber 106 of the pump cylinder 104. The fluid flow of saline S1 is identified by arrow A4 in FIGS. 35-36.

[00180] As will be clear from the foregoing, retraction of the plungers 200 in the pump chambers 106 of the respective pump cylinders 104 results in fluid being drawn into the

corresponding inlet manifold channel 236 to act upon the inlet check valves 194. The fluid flow acts upon the inlet check valves 194 and the inlet check valves 194 regulate the fluid flow into the pump chambers 106 of the pump cylinders 104. When the pressure in the inlet manifold channel 236 is greater than the pressure within the pump chambers 106 of the pump cylinders 104, such as when the plungers 200 are retracted in the pump cylinders 104, the inlet check valves 194 deform to allow fluid flow into the pump chambers 106. When the pressure within the pump chambers 106 of the pump cylinders 104 is greater than the pressure within the inlet manifold channel 236, such as when the plungers 200 are moving forward or distally within the pump cylinders 104, the inlet check valves 194 are pressed against the check valve recesses 252 formed in the rear or proximal side 234 of the manifold plate 230, and prevent fluid flow out of the pump cylinders 104 into the corresponding inlet manifold channel 236.

[00181] As fluid enters the pump chamber 106 of the pump cylinder 104 via the inlet opening 142 as the plunger 200 is retracted within the pump cylinder 104, the fluid enters the front pumping zone 164 of the pump cylinder 104. The rear isolation zone 166 of the pump cylinder 104 is present for sterility purposes, as described previously. The inner diameter of the pump cylinder 104 in the area of pumping zone 164 is desirably slightly smaller than the inner diameter of the pump cylinder 104 in the area of the isolation zone 166. The larger inner diameter of the pump cylinder 104 in the area of the isolation zone 166 serves as a storage location for the plunger 200 prior to use and prevents the front lip seal 218 from being compressed and permanently deformed during long-term storage. This storage configuration is shown in FIG. 30, discussed previously. During use, the front lip seal 218 remains within the front pumping zone 164 of the pump cylinder 104 and the rear bead seal 220 remains in the rear isolation zone 166. Since the two (2) seals 218, 220 do not contact the same surfaces, the potential for contamination from the ambient environment is reduced.

[00182] For each of the inlet selector valves 300, the rearmost saline port 334 on the inlet selector valve cylinder 114 is located near the rear or proximal end opening 120 and, accordingly, located near the proximal end of the axial passage 310 in the valve stem 306 of the inlet selector valve body 302 to allow substantially the entire valve 300 to be primed using saline. During priming, air is pushed by the priming saline from the rear of the selector valve 300 down the length of the axial passage 310 in the valve stem 306 and into the associated inlet manifold channel 236 and into the pump chambers 106 of the associated pump cylinders 104. Desirably, the axial passage 310 in the valve stem 306 is generally horizontal rather than oriented at an angle or having a slope, which enhances air bubble

removal. However, if desired, the axial passage 310 in the valve stem 306 may generally slope upward toward the corresponding inlet manifold channel 236 to aid in air removal from the valve stem 306. The inlet selector valve cylinder 114 and valve stem 306 of the inlet selector valve 300 are also generally parallel to the corresponding pump cylinders 106. As a result of the foregoing arrangement and priming sequence, stagnation regions or "dead areas" are minimized in the inlet selector valve cylinder 114 and in the axial passage 310 in the valve stem 306, minimizing the potential for trapped air bubbles. Saline S1 or saline S2 contained in the fluid source containers 30 may be used for priming of the pump 10 with fluid. As saline is much less expensive than most therapeutic or diagnostic (e.g., pharmaceutical) fluids, it is preferred for priming operations for the pump 10. After a fluid injection or infusing procedure involving a therapeutic or diagnostic (e.g., pharmaceutical) fluid has occurred, it may be desirable to flush the contents of the pump chambers 106 of the pump cylinders 104 from the pump 10, and the saline S1, S2 in the connected fluid source containers 30 may be used for this purpose. This "saline" flushing step also desirably flushes residual fluids in the flow paths upstream and downstream from the pump cylinders 104. Referring to FIGS. 29A – 29H, the inlet ports 322-328 in the valve stem 306 of [00183] the inlet selector valves 300 are desirably placed at respective angular locations to minimize "cross-over" of unprimed inlet ports 122, 124 or an unprimed port 332, 334 connected to the saline manifold 130. In practice, the rearmost saline port 334 is primed first with saline as the first installed fluid source container 30 is a saline fluid source container 30 that is installed in the left rear position on the pump 10, and minimization of "cross over" is primarily a concern with respect to inlet 122, 124 and saline port 332. Crossing over an unprimed port can undesirably introduce air into the axial passage 310 in the valve stem 306 of the selector valve 300. Accordingly, the rearmost saline channel 134 of the saline manifold 130 is supplied by the saline source S1 connected to the saline port 126 located on the left side 18 of the pump 10 and delivers saline to rearmost inlet port 328 on both the left and right inlet selector valves 300. Next, the forward saline channel 132 is supplied by the saline source S2 connected to the saline port 126 located on the right side 16 of the pump 10 and delivers fluid to the next-to-rearmost inlet port 326 on both the left and right inlet selector valves 300. The inlet ports 322-328 are located so that the valve stem 306 may be moved from a position permitting fluid communication between the rearmost inlet port 328 and the saline port 334 to the saline channel 134 connected to the left side saline fluid source containers 30 containing saline "S1" and the "OFF" position of the valve stem 306, without any of the remaining inlet ports 322-326 crossing over any of the inlet ports 122, 124 of the inlet selector valve cylinder

114 or the forward saline port 332 leading to the saline channel 132 of the saline manifold 130. Accordingly, the valve stem 306 may be rotated from any inlet port 122, 124 with an installed or connected fluid source and any saline port 332, 334 with an installed or connected saline source S1, S2 to any other such port with an installed or connected fluid source without crossing over an unprimed inlet port. FIGS. 29A-29H show several exemplary scenarios showing how the angular positioning of the inlet ports 322-328 prevents "cross-over" of unprimed fluid ports.

[00184] In FIG. 29A, the valve stem 306 of the inlet selector valve 300 is shown at an "OFF" position and a saline fluid source container 30 containing saline S1 has been installed, primed, and is ready for use as the first "saline" port S1. As shown in FIG. 29B, the valve stem 306 may be rotated between the OFF position and the first saline port S1 without having to pass over any unprimed ports, such as ports A1, A2, or S2, as discussed herein. If the valve stem 306 passes over an unprimed port, it is possible for air to be introduced into the axial passage 310 in the valve stem 306 of the inlet selector valve 300. This air could eventually be delivered to the patient outlet port 270 and to the patient unless the fluid injection is aborted by the control system 800. As shown by FIGS. 29A-29B, the first saline port S1 is always desired to be the first primed port because if the second saline port S2 was primed before the first saline port S1, the valve stem 306 would be forced to pass over the unprimed first saline port S1.

[00185] FIGS. 29C and 29D show the inlet selector valve 300 after the first saline port S1 and a first "contrast" port A1 have been installed, primed, and are ready for use. Again, in this situation, the valve stem 306 may be freely rotated from the first saline port S1, past the OFF position, and to the first contrast port A1 without having to pass over any unprimed ports, such as ports A2 or S2. Again, if the second "contrast" port A2 had been primed with fluid before the first contrast port A1, the valve stem 306 of the inlet selector valve 300 would have to pass over the unprimed first contrast port A1. For this reason, the fluid source containers 30 should be loaded in a specific order as outlined herein. In brief, the first saline source S1 should be installed before the second saline source S2, the first "medical" fluid source A1 should be installed before the second such source A2, etc.

[00186] FIGS. 29E and 29F show the inlet selector valve 300 after the fluid source container 30 containing the first contrast source A1 has run empty and the fluid source container 30 containing the second contrast source A2 has been installed. When the fluid source container 30 containing the first contrast source A1 runs empty, an air detector (described herein) associated with the connected fluid supply tube 34 alerts the control

system **800**, which actuates the drive and actuating system **400** to stop using the fluid source container **30** before any air can be drawn into the inlet selector valve **300**. Thus, the fluid supply tube **34** connected to the fluid source container **30** containing the first contrast source **A1** remains primed even though the fluid source container **30** is now empty. The valve stem **306** may be moved from the first saline port **S1**, past the OFF position, past the still-primed first contrast port **A1**, and to the second, primed contrast port **A2** without having to pass over an unprimed port, such as the second saline port **S2**. Even though the fluid supply container **30** connected to the first contrast port **A1** is now empty, the valve stem **306** can still pass over this port because the connected fluid supply tube **34** remains primed with fluid.

[00187] FIGS. 29G and 29H show the inlet selector valve 300 after the fluid source containers 30 containing the first saline source S1 and the first contrast port A1 have run empty and the fluid source container 30 containing the second saline source S2 has been installed. Again, in a similar manner to the foregoing, the first saline port S1 and the first contrast port A1 remain primed even though their respective fluid source containers 30 have run empty. If the valve stem 306 is initially located at the second saline port S2, it may be safely moved past the first saline port S1, the OFF position, and the first contrast port A1 ports to access the second contrast port A2.

[00188] As will be clear from all the foregoing, fluid as selected by the inlet selector valve **300** enters the associated inlet manifold channel **236** via the corresponding or registering openings **118**, **240** in the front plate **102** of the pump body **100** and in the manifold plate **230**. The left and right inlet manifold channels **236** are located low across the manifold plate **230** below the outlet manifold channel **244** to allow trapped air to rise upward and into the pump chambers **106** of the respective pump cylinders **104** during saline priming. The inlet manifold channels **236** are also formed with smooth interior surfaces and curvatures to avoid "dead ends" to minimize the potential for trapped air bubbles and to allow fluids to be easily flushed from the pump **10**. Moreover, the width and height of the inlet manifold channels **236** are sized and shaped to minimize the pressure drop (*e.g.*, flow restriction) while keeping the total enclosed volume to a minimum to minimize the volume of fluid required to prime the pump **10**. Fluid from the inlet selector valve **300** is available to either or both of the pump cylinders **104** on the same side of the pump **10**.

[00189] Referring further to FIGS. 37-39, during the forward or distal movement of the plunger 200 in the pump chamber 106 of the pump cylinder 104, pressure within the pump chamber 106 of the pump cylinder 104 is greater than the pressure in the outlet manifold channel 244, and the outlet check valve 196 associated with the pump cylinder 104 deforms

to allow fluid flow from the pump cylinder 104. Accordingly, in the example described previously, the pump chamber 106 of the right outboard pump cylinder 104 contains a fluid mixture comprising diagnostic or therapeutic (e.g., pharmaceutical) fluids **B1**, **B2** and saline S1, S2. As the plunger 200 in the right outboard pump cylinder 104 is moved forward or distally in the pump cylinder 104, pressure within the pump chamber 106 is greater than the pressure in the outlet manifold channel 244 and the outlet check valve 196 associated with the right outboard pump cylinder 104 deforms to allow a fluid flow of the fluid mixture comprising fluids B1, B2 and saline S1, S2 to exit the right outboard pump cylinder 104 via the air egress opening 160 and outlet openings 162 present in the distal end wall 110 of the pump cylinders 104, and enter the outlet manifold channel 244. The fluid flow of the fluid mixture comprising fluids B1, B2 and saline S1, S2 from the pump chamber 106 to the outlet manifold channel 244 is identified by arrow A₅ in FIGS. 38-39. The outlet manifold channel 244 collects the fluid ejected from each of the four (4) pump cylinders 104 and directs the combined fluid flow via the connecting passage 268 leading to the outlet selector valve 280 and the flow passage 290 therein. Accordingly, in the foregoing example, the fluid flow of the fluid mixture comprising fluids B1, B2 and saline S1, S2 is delivered under pressure into the outlet manifold channel 244 and enters the connecting passage 268 leading to the flow passage 290 in the outlet selector valve 280. The outlet selector valve 280 may selectively direct the fluid mixture to the patient outlet port 270 having the patient supply set 40 connected thereto, or to the waste outlet port 272 having the waste collection system 44 connected thereto.

[00190] Conversely, when the pressure in the outlet manifold channel 244 is greater, such as when the plunger 200 is retracted in the pump cylinder 104, the outlet check valve 196 associated with the pump cylinder 104 is pressed into the recessed area 158 defined in the elongated recess 154 on the front side 140 of the front plate 102 to seal the outlet openings 162 and top opening 160 in the front plate 102 leading to the pump chamber 106 of the pump cylinder 104 and prevents fluid flow from the outlet manifold channel 244 into the pump cylinder 104. This result occurs for each of the outlet check valves 196 to prevent fluid flow from the respective pump cylinders 104 when the corresponding plunger 200 is retracted in the pump chamber 106 of the pump cylinder 104.

[00191] The outlet check valves 196 regulate the fluid flow from each pump cylinder 104. Because pressure restrictions are not a significant concern on the outlet side of the pump 10, the one or more outlet openings 162 and the top opening 160 to each of the pump cylinders 104 may be small in comparison to the inlet openings 142 to the pump cylinders 104 to

reduce the pressure stresses on the corresponding outlet check valves 196. Additionally, the preload pins 250 in the outlet check valve receiving recesses 246 located in outlet manifold channel 244 apply a relatively high force to the outlet check valves 196, which causes the valves 196 to have a relatively high cracking pressure and help prevent free-flow due to gravity from the fluid source containers 30 to the outlet selector valve 280. The compression of the preload pins 250 and the thickness of the polymeric discs comprising the outlet check valves 196 may be optimized to prevent free-flow due to gravity from the fluid source containers 30 to the outlet selector valve 280. The preload pins 250 apply a biasing or preload force to the polymeric discs comprising the outlet check valves 196 so that a certain minimum fluid pressure, often termed "cracking pressure", is required to cause the polymeric disc to initially open. Generally, the fluid source containers 30 as associated with the pump 10 are located at a higher elevation than the location where the patient supply set 40 connects to the pump 10, namely, the patient outlet port 270. Accordingly, there is a possibility that fluid could flow under gravity alone from the fluid source container(s) 30 to the patient when the pump 10 is not operating. To prevent this situation, the preload on the outlet check valves 196 may be made high enough that their cracking pressure is greater than this head pressure. The outlet manifold channel 244 collects the fluid ejected from each of the four [00192] (4) pump cylinders 104 and directs the combined fluid flow to the outlet selector valve 280. The outlet selector valve 280 allows the fluid output to be directed to either patient outlet port 270 having the patient supply set 40 connected thereto, or to the waste outlet port 272 having the waste collection system 44 connected thereto. As noted previously, the valve stem 286 may be rotated to one of three (3) possible positions, including: (1) placing the flow passage 290 in fluid communication with the patient outlet port 270; (2) placing the flow passage 290 in fluid communication with the waste outlet port 272; and (3) placing the flow passage 290 in a shut-off position wherein flow to either the patient outlet port 270 or the waste outlet port **272** is prevented.

[00193] As noted previously, the manifold plate 230 is laser welded to the front plate 102 of the pump body 100 to secure these two components together and form a hermetic seal around critical fluid path areas. Because the outlet manifold channel 244 is generally under high pressure, for example, at least 400 psi and, often, at least 500 psi and greater, the welded seam in the perimetrical recess 156 around the outlet manifold channel 244 may not be fully capable of repeatedly withstanding the high stresses while maintaining a hermetic seal. To reduce the stress on this particular welded joint, the drive and actuating system 400 includes a spring-loaded clamp (described herein) to apply several hundred pounds of force to the rear

side of the front plate **102** of the pump body **100** and allows the pump **10** to withstand fluid pressure of at least 400 psi and, desirably, at least 500 psi and greater. This clamping force likewise prevents separation of the laser weld joint or joints between the front plate **102** of the pump body **100** and the manifold plate **230**.

[00194] As previously noted, various versions and embodiments of the fluid supply set 32 may be associated with the pump 10 to meet different patient and/or procedural needs, as described herein. The combination of the pump 10 and a specific configuration of the fluid supply set 32 forms the multi-use or multi-patient disposable set for the fluid delivery system or unit 2. Referring further to FIGS. 40-43, each of the various versions and embodiments of the fluid supply set 32 comprises one or more fluid supply tubes 34 each having one end connected to the pump 10 and the opposing end connected to a spike 36 used to access a fluid source container 30. In certain variations or configurations, the fluid supply set 32 may allow the fluid source containers 30 to be replaced without contamination of the pump 10.

[00195] A "basic" embodiment of the fluid supply set 32 is shown in FIG. 40. The basic fluid supply set 32 comprises six (6) fluid supply tubes 34 which connect six (6) fluid source containers 30 to the six (6) inlet ports 122, 124, 126 on the inlet selector valve cylinders 114 on the pump body 100. The basic configuration is for a typical end user performing, for example, 8-12 procedures per day and be may be used, for example, on up to about 15 patients. In this configuration, two (2) contrast fluid source containers 30 containing contrast fluids A1, A2, for example, the same type or brand of contrast fluid, may be connected to the first and second inlet ports 122, 124 on the left side inlet selector valve cylinder 114, and two (2) contrast fluid source containers 30 containing contrast fluids B1, B2, for example, the same type or brand of contrast fluid but different from contrast fluids A1, A2, may be connected to the first and second inlet ports 122, 124 on the right side inlet selector valve cylinder 114. However, if desired, the same type of fluid may be present in all four (4) of the foregoing installed fluid source containers 30. Fluid source containers 30 containing saline S1, S2 are connected to the saline ports 126 on each of the inlet selector valve cylinders 114 in the manner discussed previously. The basic fluid supply set 32 typically has permanently attached spikes 36 on the free end of each of the fluid supply tubes 34, and the other end of each of the fluid supply tubes 34 is permanently connected to the respective inlet ports 122, 124, 126. However, one or more of the spikes 36 may be replaceable spikes if so desired. For example, replaceable spikes 36 may be provided for accessing the saline fluid source containers 30 containing saline S1, S2. Once the fluid source container 30 attached to each spike 36 is empty, that particular fluid supply tube 34 and the associated inlet port 122, 124,

126 should no longer be used because of the contamination risk involved in changing out a fluid source container **30**.

[00196] In FIG. 41, a "high-use" fluid supply set 32 is shown and differs only from the basic configuration in that all the spikes 36 are replaceable. A swabable valve 70 may be provided on the free end of the fluid supply tubes 32 for connection to the spikes 36. In this variation, one fluid source container 30 may be attached to each spike 36 and, once empty, the empty container 30 and used spike 36 may be removed and discarded. The permanently attached swabable valve 70 may then be cleaned and a new spike 36 attached to the valve 70. Multiple fluid source containers 30 may be installed on a given fluid supply set 32 as long as the spike 36 is replaced with each new container 30 and the corresponding swabable valves 70 are cleaned appropriately.

[00197] In FIG. 42, another variation of the fluid supply set 32 is shown and intended for limited use with only a few patients, such as may occur on a weekend. This variation of the fluid supply set 32 may be used, for example, on up to about five (5) patients and has a single fluid source container 30 containing a desired therapeutic or diagnostic (e.g., pharmaceutical) fluid connected to one of the first inlet ports 122 on the left or right side inlet selector valve cylinders 114. A saline fluid source container 30 containing saline is connected to the saline port 126 on the same inlet selector valve cylinder 114. The spikes 36 are shown permanently attached to fluid supply tubes 34 so once a fluid source container 30 is empty, that particular fluid supply tube 34 and inlet port 122, 126 should no longer be used. However, swabable valves 70 may also be used in the manner shown in FIG. 41.

[00198] In FIG. 43, a further variation of the fluid supply set 32 is shown and is intended for use with small, single-patient fluid source containers 30. This variation is intended to be used, for example, for up to about 15 patients. In this variation, a first type of therapeutic or diagnostic (e.g., pharmaceutical) fluid A1 in a fluid source container 30 is connected to the first inlet port 122 on one of the inlet selector valve cylinders 114, and a second type of therapeutic or diagnostic (e.g., pharmaceutical) fluid B1 is connected to the first inlet port 122 on the other inlet selector valve cylinder 114. Saline S1 in a fluid source container 30 is connected to the saline port 126 on one of the inlet selector valve cylinders 114. In this variation, swabable valves 70 are provided on the free ends of the fluid supply tubes 32 for connection to replaceable spikes 36. Accordingly, once the fluid source container 30 attached to the respective spikes 36 is empty, the empty container 30 and used spike 36 may be removed and discarded. The permanently attached swabable valve 70 may then be cleaned

and a new spike **36** may be attached to the valve **70**, along with a new fluid source container **30**.

[00199] As shown in FIG. 44, the single-patient supply set 40 generally comprises medical tubing having opposed free ends each with a fluid connector 42. The patient-end fluid connector 42 is used to make a fluid connection to a catheter inserted into a patient to convey a desired fluid or mixture of fluids to a desired location within the patient's body. The patient-end fluid connector 42 may include a check valve (not shown) to prevent reverse flow from the patient. The other free end fluid connector 42 is connected to the patient outlet port 272 on the outlet selector valve cylinder 264 on the manifold plate 230.

[00200] Further, FIG. 45 shows the waste collection system 44 associated with a pump 10 having a "high-use" fluid supply set 32. As described previously, the waste collection system 44 generally comprises a waste collection tube set 46 connected to a waste collection container 48 used to collect and store waste fluids. The waste collection tube set 46 is adapted to make a fluid connection with the pump 10. In particular, the waste collection system 44 is connected to the waste outlet port 272 on the outlet selector valve cylinder 264 on the manifold plate 230, as noted previously, and the waste collection tube set 46 conducts waste fluids to the waste collection container 48 when the outlet selector valve 280 is actuated to place the flow passage 290 in fluid communication with the waste outlet port 272. A check valve (not shown) may be incorporated into the fluid connector on the waste collection tube set 46 which prevents accidental reverse flow from the waste collection container 48 into the pump 10. Additionally, if the waste collection container 48 is removed and replaced with a new waste collection container 48, the check valve prevents the contents of the full waste collection container 48 from being ejected during handling.

[00201] As noted in the foregoing, the fluid delivery system 2 comprises a drive and actuating system 400 that interfaces with the pump 10 to provide the motive forces for operating the various components of the pump 10. Referring next to FIGS. 46-60, details of the drive and actuating system 400 will be described. The drive and actuating system 400 is supported by a mobile support or superstructure 700 that also supports a fluid management system 720 for supporting, maintaining, and monitoring the various diagnostic or therapeutic (e.g., pharmaceutical) fluids to be associated with the pump 10. Particularly, the fluid management system 720 provides air management functions for the fluid delivery system 2, as described herein in connection with FIG. 60. The mobile support or superstructure 700 permits the fluid delivery system 2 to be a mobile system for applications in various medical environments, such as medical imaging suites that utilize a computed tomography (CT)

scanner, as an example. As a result, the fluid delivery system 2 may be positioned in close proximity to the patient during a fluid injection and scanning procedure and a "short" patient supply set 40 may be used. Additionally, depending upon the type of procedure being performed, it may be desirable to place the fluid delivery system 2 either in front of the CT scanner gantry or behind the gantry. This placement is typically determined by whether the scan is being performed with the patient's hands/arms above their head for chest and abdominal scans, or at their sides for head and neck scans. Further, the system 2 may easily be moved out of the way to permit the patient to be placed on or removed from the bed of the CT scanner. Furthermore, the fluid delivery system 2 includes a control system 800, as noted previously, for coordinating and controlling operation of the various components and functions of the drive and actuating system 400 and fluid management system 720, each supported on the mobile support 700.

[00202] FIG. 47 is a block schematic representation of the drive and actuating system 400 of the fluid delivery system 2. Generally, the drive and actuating system 400 comprises a movable pump drawer section 402 that is extendable and retractable on the mobile support 700 to allow loading/unloading of the pump 10 into/from the pump drawer 402. The drive and actuating system 400 also comprises a drive section 440 that generates the motive forces for reciprocal operation of the pistons 50 operating the respective plungers 200 and rotational operation of the inlet selector valves 300. Additionally, the drive and actuating system 400 comprises a drive interface section 460 that translates and/or transmits the motive forces from the drive section 440 to the pistons 50 and inlet selector valves 300. Further, the drive and actuating system 400 comprises a pump clamping section 520, also referred to herein as a pump clamping mechanism 520, that secures the pump 10 in association with the drive and actuating system 400. Furthermore, the drive and actuating system 400 comprises an outlet selector valve actuating section 580 that operates the outlet selector valve 280 on the pump 10. The drive and actuating system 400 desirably further supports several components of the control system 800, including a drive control board 802 that is electronically connected and interfaced with the control system 800 to enable the control system to control operation of the drive section 440, and a sensor control board 804 used to collect sensor information from various sensors in the drive and actuating system 400 and relay this electronic information to the control system 800 to enable the control system 800 to control operation of the drive section 440, drive interface section 460, pump clamping mechanism 520, and outlet selector valve actuating section 580. Each of the foregoing sections is described hereinafter in connection with FIGS. 46-60.

[00203] The pump drawer 402 is generally extendable and retractable from the mobile support 700 and comprises a drive and actuating support structure 420 that mounts and supports the various components of the drive section 440, drive interface section 460, pump clamping section 520, and outlet selector valve actuating section 580. The pump drawer 402 includes a handle housing portion 404 and a waste collection compartment 406 to accommodate the waste collection container 48 and at least portions of the associated waste collection tubing set 46, which were described previously. The handle housing portion 404 is supported by a composite drawer support structure 408 that is mechanically affixed to a drawer shelf plate 410. The handle housing portion 404 is mounted to the drawer support structure 408 so that the handle housing portion 404 forms a portion of the cosmetic outer face of the pump drawer 402.

[00204] A pump cradle 412 is fixedly mounted on the top side of the drawer shelf plate 410 to support and maintain the pump 10 on the drawer shelf plate 410. The pump cradle 412 is preformed to the shape of the pump 10 to secure the pump 10 in the pump drawer 402 and comprises preformed cradle appendages 414 to interface with the fluid supply tubes 34 of the various embodiments of the fluid supply sets 32 described previously. The cradle appendages 414 are formed for easy loading of the pump 10 in the pump drawer 402. The handle housing portion 404 may be a singular component or a composite structure, as indicated above, that includes a reinforcing and locking support plate 416 sandwiched between two face plates 418. A drawer handle H is formed integrally on the outside face of the handle housing portion 404 to enable a user to slidably operate the pump drawer 402. The waste collection compartment 406 may be detachably suspended from lateral sides of the drawer shelf plate 410. The locking support plate 416 may be made of metal such as stainless steel or another metal suitable for applications in medical environments, and the face plates 418 may be polymeric covering face plates that have suitability for improving the ornamental or cosmetic exterior appearance of the pump drawer 402.

[00205] The drive and actuating support structure 420 comprises a rear support plate 422 that supports a top, distally-extending support plate 424 and a bottom, distally-extending support plate 426. The drawer shelf plate 410 of the pump drawer 402 is journalled for slideable movement relative to the bottom support plate 426 by a pair of mounting flanges 428 mounted on opposing sides of the top side of the bottom support plate 426. A drive enclosure or housing 430 may be secured to the bottom support plate 426 to enclose a region forward or distal of the rear support plate 422 and below the bottom support plate 426. The drive enclosure 430 encloses the various drive motors of the drive section of the drive and

actuating system **400** as well as the drive control board **802**, as described herein. A base plate **432** may be connected to or extend from the lower end of the rear support plate **422** to support the drive control board **802**, and support rods may extend from the drive control board **802** to the bottom support plate **426** for rigidity purposes. An intermediate support plate **434** is located on top of the bottom support plate **426** and forward of the rear support plate **422** to support the drive pistons **50** and actuator components used to operate the inlet selector valves **300**, as described hereinafter. Several support openings **436** are provided in the intermediate support plate **434** for the drive pistons **50** and the actuator components used to operate the inlet selector valves **300**. Support elements **438** are provided in each of the support openings **436** in the intermediate support plate **434** to support the drive pistons **50** and actuator components used to operate the inlet selector valves **300**. These support elements **438** may be bushings in the case of the drive pistons **50** and support ball bearings in the case of the actuator components.

As noted in the foregoing, the drawer shelf plate 410 of the pump drawer 402 is journalled for slideable movement relative to the bottom support plate 426 by a pair of mounting flanges 428 mounted on opposing sides of the top side of the bottom support plate **426**. This slideable movement permits the pump drawer **402** to move from a closed position in which the pump drawer 402 is received within the mobile support 700 to an extended position outward from the mobile support 700 to permit a user to load a pump 10 into the pump cradle 412. The handle H on the handle housing portion 404 is used by the user to extend and close the pump drawer 402. The sliding movement of the drawer shelf plate 410 enables the handle housing portion 404 and the waste collection compartment 406 depending from the drawer shelf plate 410 to be moved together as a singular unit from the closed or retracted position of the pump drawer 402 to the extended or loading position of the pump drawer 402. The pair of mounting flanges 428 mounted on opposing sides of the top side of the bottom support plate 426 support the drawer shelf plate 410 in both the extended or loading position of the pump drawer 402 and the closed or retracted position of the pump drawer 402 and an extension limiter may be provided so that the drawer shelf plate 410 cannot be extended to a point where the pump drawer 402 disengages entirely from the mounting flanges 428. As described further herein, a locking connection may be provided between the locking support plate 416 and the drive and actuating support structure 420 to lock the pump drawer 402 in the closed position so that the pump 10 is secured during operation of the fluid delivery system 2.

[00207] The drive section 440 comprises, in the present embodiment, four (4) piston actuator drive motors 442, such as servomotors and the like, that provide the motive forces which drive four (4) respective piston linear actuators 462 that individually operate the drive pistons 50. Additionally, the drive section 440 comprises a pair of inlet selector valve actuator drive motors 444, such as stepper motors and the like, that provide the motive forces which drive a pair of inlet selector valve actuators 464 that independently operate the respective inlet selector valves 300, as also described herein. The piston drive motors 442 are mounted to the front or distal facing side of the rear support plate 422 beneath the bottom support plate 426 and each have a drive shaft 446 extending through an opening in the rear support plate 422 to output motive forces to the piston linear actuators 462. Likewise, the respective inlet selector valve drive motors 444 are mounted to the front or distal facing side of the rear support plate 422 beneath the bottom support plate 426 and each have a drive shaft 448 extending through an opening in the rear support plate 422 to provide motive forces to the inlet selector valve actuators 464. The respective drive motors 442, 444 are electronically controlled by the control system 800 via respective electronic connections 450 with the drive control board 802. A drive pulley 452 is mounted to the drive shaft 446 of each of the piston drive motors 442 and, likewise, a drive pulley 454 is mounted to the drive shaft 448 of each of the inlet selector valve drive motors 444. As will be appreciated from the foregoing, a piston drive motor 442 is provided for each of the drive pistons 50 and an inlet selector valve drive motor 444 is provided for each of the inlet selector valves 300 based on the pump 10 comprising four (4) separate pump cylinders 104 and two (2) separate inlet selector valves 300. However, as noted previously, this exemplary configuration should not be deemed limiting as other configurations with a fewer or increased number of pump cylinders 104 and inlet selector valves 300 may be desirable for the fluid delivery system 2.

[00208] As mentioned in the foregoing, a locking connection is desirably provided between the locking support plate 416 and the drive and actuating support structure 420 to lock the pump drawer 402 in the closed position so that the pump 10 may be secured during operation of the fluid delivery system 2 or at other suitable times. This locking connection may be provided by a series of locking teeth 456 on the upper end or edge of the locking support plate 416 that engages a corresponding series of locking slots 458 provided in a front or distal end 508 of the opposing top support plate 424. The locking slots 458 may define a generally L-shaped configuration to receive the locking teeth 456. The locking support plate 416 is sandwiched and supported between the two opposing face plates 418 so as to be capable of limited lateral, side-to-side movement between the face plates 418. This limited

lateral, side-to-side movement enables the locking teeth 456, after having engaged the L-shaped locking slots 458, to be placed into the transversely extending or "dog leg" of the locking slots 458 from a longitudinal or entry leg of the locking slots 458 by limited lateral movement of the locking support plate 416. The movement of the locking teeth 456 into the transversely extending portion or "dog leg" of the locking slots 458 places the pump drawer 402 into a locked position or state. A similar set of "lower" locking teeth (not shown) to the "upper" locking teeth 456 may be provided on the bottom of the locking support plate 416 to engage similar "lower" locking slots (not shown) to the "upper" locking slots 458 provided in the bottom support plate 426.

[00209] The locking slots 458 generally oppose the locking teeth 456 so that when the pump drawer 402 is moved by the user to the closed or retracted position, the locking teeth 456 are automatically engaged in the longitudinal or entry legs of the locking slots 458. A lock actuator (not shown), such a cam mechanism, may be provided to actuate the locking support plate 416 between the foregoing locked position (e.g., in which the locking teeth 456 engage a transversely extending portion of the locking slots 458) and the release or unlocked position in which the locking teeth 456 are aligned with the longitudinal or entry leg of the locking slots 458 that are aligned with the locking teeth 456. A drawer closed sensor 818 is provided on the top support plate 424 to determine the presence of the locking teeth 456 in the locking slots 458. The drawer closed sensor 818 is electronically coupled to the sensor control board 804 and, thereby, the control system 800 can determine when the locking teeth **456** are engaged in the locking slots **458** and whether the lock actuator should be actuated to move the locking support plate 416 laterally into a locking engagement with the transversely extending portion of the locking slots 458 so the locking support is locked with the top and bottom support plates 424, 426, or unlocked from the top and bottom support plates 424, 426 so that the pump drawer 402 may be opened for loading or removal of the pump 10.

[00210] As noted in the foregoing, a lock actuator (not shown), such as a cam mechanism, may be associated with the locking support plate 416 to move the locking support plate 416 between the locked and unlocked positions. The cam mechanism may be operated or actuated by extension and retraction of one of the two (2) inboard piston linear actuators 462, described herein, and, typically, the left inboard piston linear actuator 462 in the embodiment of the drive and actuating system 400 shown in FIGS. 47-59. The operation of the left inboard piston linear actuator 462 moves the cam mechanism to move the locking support plate 416 between the locked and unlocked positions, which locks and unlocks the pump drawer 402. For example, retraction of one of the inboard piston linear actuators 462,

typically, the left inboard piston linear actuator 462, moves the cam mechanism to move the locking support plate 416 laterally to the unlocked position, which unlocks the pump drawer **402.** The pump drawer **402** has right and left sides corresponding to the right and left sides 16, 18 of the pump 10. The user may then open the pump drawer 402 and insert the pump 10 into the pump drawer 402. The user may then close the pump drawer 402. Once the pump drawer 402 is closed, the control system 800 is so alerted by the drawer closed sensor 818, as noted in the foregoing, and may actuate the left inboard piston linear actuator 462 to move the locking support plate 416 to lock the pump drawer 402. In particular, the control system 800 detects that the pump drawer 402 is closed via the drawer closed sensor 818 and operates the drive motor 442 associated with the left inboard piston linear actuator 462 to move the left inboard piston linear actuator 462 slightly forward to actuate the cam mechanism to move the locking support plate 416 laterally to the locked position. The control system 800 confirms that the pump drawer 402 has been locked with a drawer locked sensor 820 provided on the top support plate 424 which may detect the shifted lateral position of the locking support plate 416. It will be appreciated that a manually-actuated locking device may be provided in place of the foregoing automated lock actuator or may be provided as an augmentation to the automated lock actuator, and have a handle or other suitable manual actuator on the exterior of the mobile support 700 for operation by the user or operator. The drawer locked sensor 820 may be used as a safety device in that, if this sensor is not tripped to indicate that the pump drawer 402 is closed, no drive motion will be permitted by the control system **800** in order to prevent possible user injury.

[00211] The drive interface section 460 is provided to convert the rotary output of the drive shafts 446 of the piston drive motors 442 into reciprocal translational motion of the drive pistons 50 and, further, transfer and translate the rotary output of the drive shafts 448 of the inlet selector valve drive motors 444 into corresponding and controlled rotational movement of the inlet selector valve actuators 464, which control the angular positioning of the respective inlet selector valves 300 and, hence, the operational state of the inlet selector valves 300. In one exemplary embodiment, the drive interface section 460 comprises four (4) piston linear actuators 462 in the form of ball screw linear actuators that convert the rotational drive output of the drive shafts 446 of the piston drive motors 442 into reciprocal translational movement of the pistons 50 so that the pistons 50 may reciprocally and independently operate the plungers 200 in the respective pump cylinders 104. In the illustrated embodiment, each ball screw-type piston linear actuator 462 comprises a ball screw shaft 466 rotationally journalled in a ball screw nut 468 by threaded engagement as is

well-known in the mechanical arts. Each ball screw nut **468** is fixedly mounted to an individual slide block **470** and may be mounted for guided sliding reciprocal movement on a support platform **472** disposed between the mounting flanges **428** on the top side of the top support plate **424** of the drive and actuating support structure **420**.

[00212] The ball screw shafts 466 each have a proximal portion 474 extending through a corresponding mounting opening 476 in the rear supporting plate 422. The proximal portion 474 of each ball screw shaft 466 is rotationally supported in the receiving mounting opening 476 by a suitable rotational, thrust support bearing 478. A support plate 480 is provided on the distal or front side of the rear support plate 422 to restrain the bearings 478 in the respective mounting openings 476. As will be understood from the view in FIG. 53, the respective pistons 50 each have a proximal end 58 and define a central or axial bore 60 opening externally at the proximal end 58. The proximal end 58 of each of the pistons 50 may have a lip or flange 62 for mounting the proximal end 58, in any desirable manner, to a corresponding slide block 470 so that reciprocal movement of the individual slide blocks 470 results in concurrently reciprocal movement of the connected drive piston 50. The proximal portion 474 of each of the ball screw shafts 466 has an actuator pulley 482 mounted thereto, and a timing belt 484 is reeved about the drive pulley 452 on the drive shaft 446 of the corresponding piston drive motor 442 and the actuator pulley 482 to rotationally interface the drive shaft 446 and the ball screw shaft 466. The pulleys 452, 482 and timing belt 484 permit the driving rotational movement of the associated drive shaft 446 to be imparted to the ball screw shaft 466 as will be understood to those skilled in the mechanical arts. As the ball screw shaft 466 rotates clockwise or counterclockwise, the ball screw nut 468 converts this rotational motion to linear reciprocal motion of the associated slide block 470 and, hence, linear motion of the connected drive piston 50. The drive pistons 50 are supported in the respective support openings 436 in the intermediate support plate 434 by the support elements 438, namely bushings, in the respective support openings 436 to support the linear reciprocal movement of the drive pistons 50 in the support openings 436.

[00213] The respective inlet selector valve actuators 464 are rotational motion actuators adapted to transfer and translate the rotary output of the drive shafts 448 of the inlet selector valve drive motors 444 into corresponding and controlled rotational movement of the inlet selector valve actuators 464 which control the angular positioning of the respective inlet selector valves 300 and, hence, the operational state of the inlet selector valves 300. The respective inlet selector valve actuators 464 comprise a selector rod 486 having a distal or actuator end 488 adapted to interface with the actuator interface head 304 on the inlet selector

valve body 302 of the corresponding inlet selector valves 300, and a proximal end 490 extending through one of the respective mounting openings 476 in the rear supporting plate **422.** The selector rods **486** are rotationally supported in the respective mounting openings 476 by a suitable rotational support bearing 492 and restrained in the respective mounting openings 476 by the same support plate 480, noted previously, used to secure the rotational, thrust support bearings 478 supporting the proximal portion 474 of the ball screw shafts 466 in the respective mounting openings 476 in the rear supporting plate 422. An electromechanical angular position sensor 494, such as a rotary encoder, is mechanically coupled to the proximal end 490 of each selector rod 486. The angular position sensor 494 is electronically linked to the control system 800 via an electronic link or connection 496 to the sensor control board 804. The angular position sensors 494 are operable to determine the specific angular orientation of the valve stem 306 of the inlet selector valve body 302 of the associated inlet selector valve 300, which is relayed to the control system 800 via the sensor control board 804. Accordingly, by controlled operation of the inlet selector valve drive motors 444 by the control system 800, the associated inlet selector valve 300 may be angularly positioned to one of the several operating positions discussed previously.

[00214] The distal end 488 of each of the selector rods 486 may be configured with engagement or interface elements 498 to interface with corresponding engagement components or structures on the actuator interface head 304 of the inlet selector valve body 302 of the selector valves 300. As discussed previously, these corresponding engagement components or structures include the proximal tab 312 and interface engagement member 314 formed on the actuator interface head 304. As mentioned previously, for safety purposes, it is desirable for the valve stem 306 to be engaged to the drive and actuating system 400 in only one particular angular orientation. Thus, the foregoing features on the actuator interface head 304 preferably require the valve stem 306 to be in one particular orientation for engagement with the engagement or interface elements 498 and this information may be encoded into the pump indicator plate 170 and/or into identifying indicia 172 on the pump body 100, described previously. The control system 800 can thereby determine the initial or preset angular orientation of the valve stem 306 in the inlet selector valve cylinder 114 and operate the inlet selector valve actuators 464 to engage the valve stem 306 in the right angular orientation. If the valve stem 306 can be engaged in more than one angular orientation, the wrong type of fluid could possibly be delivered to the patient. The wrong type of fluid could be delivered because, with more than one angular engagement orientation, there would no longer be a uniquely-predefined relationship between the angular position sensor 494 and the actual

position of the valve stem **306** of the inlet selector valve **300**, and the control system **800** could cause the inlet selector valve **300** to be oriented in an unintended position whereby an unintended fluid is delivered by the pump **10**.

The respective selector rods 486 are supported in the support openings 436 in the intermediate support plate 434 to permit free rotational movement of the selector rods 486. As noted previously, a support element 438, such as a bushing, is provided in each of the support openings 436 in the intermediate support plate 434 that support the linear reciprocal movement of the drive pistons 50. In the case of the selector rods 486, the support elements 438 are support ball bearings that facilitate the rotational motion of the respective pair of selector rods 486. The proximal end 490 of each of the respective selector rods 486 has an actuator pulley 500 mounted thereto, and a timing belt 502 is reeved about the drive pulley 454 on the drive shaft 448 of the driving inlet selector valve drive motor 444 and the actuator pulley 500 to rotationally interface the drive shaft 448 and the selector rod 486. The pulleys 454, 500 and timing belt 502 permit the driving rotational movement of the associated drive shaft 448 to be transferred and imparted to the associated selector rod 486. As the drive shaft 448 rotates clockwise or counterclockwise, the pulleys 454, 500 and timing belt 502 transmit the rotary motion to the selector rod 486 so that the corresponding inlet selector valve 300 may be angularly positioned to one of the several operating positions discussed previously, or any angular position programmed into the control system 800. The pulleys 454, 500 and timing belt 502 permit controlled rotational movement of the drive shaft 448 to be transferred and imparted to the associated selector rod 486, while the angular position sensor 494 continuously monitors the angular position of the selector rod 486 and, hence, enables the control system 800 to determine and control the specific angular orientation of the valve stem 306 of the inlet selector valve body 302 of the associated inlet selector valve 300. The actuator pulley 500 on the proximal end 490 of each of the respective selector rods 486 may be secured to the selector rod 486 via a suitable mechanical fastener arrangement and the respective angular position sensors 494 may be supported for mechanical connection to the proximal end 490 of the respective selector rods 486 by a support bracket mounted to the rear or proximal side of the rear support plate 422. The respective slide blocks 470, discussed previously, also each define a tapered top end portion 504, the use of which is discussed herein.

[00216] As noted previously, the pump clamping section or mechanism 520 of the drive and actuating system 400 secures the pump 10 in association with the drive and actuating system 400. The top support plate 424 generally defines a proximally extending portion or

slot **512** extending rearward or proximally from the front or distal end **508** of the top support plate **424**. The proximally extending slot **512** includes opposed interior ledges **514** along the walls of the proximal slot **512** which support certain components of the pump clamping section or mechanism **520**, as described herein. A series of elongated apertures **516** are also provided in the top support plate **424** forward or distal of the proximal end of top support plate **424** to allow the top end portions **504** of the slide blocks **470** to project upward through the top support plate **424** and, additionally, for guiding the sliding reciprocal movement of the slide blocks **470** relative to the upper support plate **424**. Accordingly, a total of four (4) elongated apertures **516** are provided in the top support plate **424** forward or distal of the proximal end of the top support plate **424**, one for each of the four (4) slide blocks **470** in the illustrated embodiment of the fluid delivery system **2**. Additionally, a pair of actuator apertures **518** is provided in the top support plate **424** distal or forward of the slide block apertures **516**, for purposes described herein.

The pump clamping section or mechanism 520 generally comprises a clamping block 522 having a front or distal end 524 and a rear or proximal end 526. A pair of guide rods 528 extends proximally or rearward from the clamping block 522. The guide rods 528 are opposed, respectively, by a corresponding pair of distally-extending guide rods 530 mounted to the front or distal side of the rear support plate 422. A pair of preloaded clamping springs 532 is mounted on the two opposing pairs of guide rods 528, 530 to apply a biasing force to the clamping block 522 in the direction of the pump drawer 402 and, particularly, the drawer support structure 408 of the pump drawer 402. The clamping block 522 is vertically supported by a series of spaced, C-shaped support appendages 534 that extend upward from the clamping block 522 to engage the opposed ledges 514 along the walls of the proximal slot 512 in the top support plate 424 so that the clamping block 522 is supported to depend below the top support plate 424. In the illustrated embodiment, a total of four (4) support appendages 534 are provided, including two (2) forward or distal support appendages 534 and two (2) rear or proximal support appendages 534. The body of the clamping block 522 is positioned below the top support plate 424 and the top support plate 424 restrains the clamping block 522 against upward movement, while the engagement of the clamping block support appendages 534 with the opposed ledges 514 along the walls of the proximal slot 512 in the top support plate 424 permits forward and rearward movement in the proximal slot 512 in the top support plate 424.

[00218] Generally, in use, when a pump 10 is loaded into the pump cradle 412 in the pump drawer 402, as described previously, the clamping block 522 is used to exert a compressive

force on the pump manifold 80 and, in particular, the rear or proximal side of the front plate 102 of the pump body 100. This compressive force is applied to the sealing element (e.g., Oring, gasket, or weld, typically a laser weld) located in the perimetrical recess 156 around the respective dish-shaped recessed areas 252 and around the outlet manifold channel 244. The compressive force seals the sealing element (e.g., O-ring, gasket, or laser or ultrasonic weld) in the perimetrical recess 156 and permits the pump manifold 80 to withstand higher pressures. As noted previously, a laser weld joint typically occupies the location of the perimetrical recess 156 in the accompanying figures, but an O-ring, gasket or like element may alternatively be provided in this location, if desired. The compressive force of the clamping block 522 similarly secures the sealing element, whether provided as a weld joint, O-ring, gasket, etc., to enable the pump manifold **80** to withstand higher operating pressures. Another feature of the pump clamping mechanism 520, and the clamping block 522 in particular, is to assist in preventing the pump 10 from moving when in use. When the respective plungers 200 are retracted in the pump cylinders 104, there is both a frictional force due to the friction between the plunger seals 218, 220 on the respective plungers 200 and the interior wall 108 of the pump cylinders 104, and a vacuum force due to the vacuum in the pump cylinders 104 during filling (e.g., retraction or withdrawal of the plungers 200 in the pump cylinders 104.) These frictional and vacuum forces "pull" the entire pump body 100 rearwards in the pump cradle 412. The pump clamping mechanism 520 acts against these frictional and vacuum forces to help hold the pump 10 in place.

[00219] The outer flange 258 and stiffening ribs 260 on the front face or side 232 of the manifold plate 230 transfer the clamping force applied by the clamping block 522 to the laser welded joint, O-ring, or gasket in the perimetrical recess 156 that is subjected to relatively high fluid pressure and stress, as well as to the other laser weld joint or joints between the manifold plate 230 and the front or distal plate 102 of the pump body 100. Additionally, the manifold caps 262 enclosing the respective right and left inlet manifold channels 236 and the stiffening ribs 260 on the front face or side 232 of the manifold plate 230 all lie substantially in the same plane so that the clamping force applied by the clamping block 522 to the manifold 80 does not deflect the front plate 102 of the pump body 100 and manifold plate 230 unevenly and/or in such a way as to damage the various laser weld joints between the manifold plate 230 and the front or distal plate 102 of the pump body 100 and, particularly, the laser weld joint in the perimetrical recess 156 that is subjected to relatively high fluid pressure and stress. This front "planar" configuration allows the clamping block 522 to prevent of the foregoing features from deflecting when subjected to high loads. Without the

clamping force applied by the clamping block **522**, the various laser welded joints and molded features of the pump body **100** and manifold plate **230** would likely have to be much stronger and stiffer.

[00220] The clamping block 522 further comprises a pair of actuator blocks 536 that extend upward through the respective lateral apertures 518 in the top support plate 424. The lateral actuator block apertures 518 are slightly larger and longer than the actuator blocks 536 to permit limited movement, in a forward or rearward direction, by the actuator blocks 536 in the actuator block apertures 518. Such movement is provided to enable a small retraction of the clamping block 522 in the proximal slot 512 in the top support plate 424 and toward the rear support plate 422 to permit loading and unloading of the pump 10 from the pump cradle 412 without having to manually retract the clamping block 522 and compress the clamping springs 532. The clamping block 522 further defines a forward lip or flange 538 provided on a top side or surface of the clamping block 522.

[00221] A clamp actuating mechanism 540 is provided to enable a small retraction of the clamping block 522 in the proximal slot 512 in the top support plate 424 and toward the rear support plate 422 to permit loading and unloading of the pump 10 from the pump cradle 412. The clamp actuating mechanism 540 is adapted to retract the clamping block 522 from engagement with the front plate 102 of the pump body 100 of the pump 10 without manual manipulation of the clamping book 522. The clamp actuating mechanism 540 comprises, for example, a pair of pivoting cam arms 542 that are pivotally connected by pivot pins 544 to the top support plate 424. The cam arms 542 are pivotally connected to the top side of the top support plate 424 outboard of the actuator blocks 536 to interface with the actuator blocks 536. The cam arms 542 comprise a first or hook end 546 that is in operative engagement with the respective actuator blocks 536 that extend upward through the respective actuator block openings 518 in the top support plate 424. The opposing second ends of the cam arms 542 are formed as cam ends 548 which contact the top end portions 504 of the slide blocks 470 of the two (2) outer or outboard slide blocks 470 that project upward through the two (2) outer or outboard slide block apertures 516 in the top support plate 424. The top end portions 504 of at least these two (2) outer or outboard slide blocks 470 comprise a tapered cam surface 550 opposing the cam ends **548** of the cam arms **542** so that rearward movement of the two (2) outer or outboard slide blocks 470 induces an outward pivotal movement of the cam arms 542 about their respective pivot pins 544. In particular, when it is desired to load or unload a disposable pump 10 from the pump cradle 412 in the pump drawer 402, the piston linear actuators 462 associated with the two (2) outer slide blocks 470 may be driven so that the

slide blocks 470 move proximally or rearward in their slide block aperture 518 toward the rear support plate 422. This proximal or rearward movement causes the tapered cam surface 550 on the top end portions 504 of the two (2) outer slide blocks 470 to contact the cam end 548 on each of the cam arms 542 and pivot the cam arms 542 about pivot pins 544. The cam ends 548 on the cam arms 542 pivot laterally outward toward the lateral outer sides of the top support plate 424 while the hook ends 546 of the cam arms 542 move the respective actuator blocks 536, extending upward from the clamping block 522, slightly rearward or proximally in their respective actuator block openings 518 in the top support plate 524 and toward the rear support plate 422 thereby slightly compressing the associated clamping springs 532. As the actuator blocks 536 move rearward or proximally, the clamping block 522 is removed from contacting compressive engagement with the pump 10 and, in particular, from compressive engagement with the rear or proximal side of the front plate 102 of the pump body 100 of the pump 10. The pump 10 may then be removed from the pump cradle 412 in the pump drawer 402 without hindrance from the clamping block 522 and replaced with a new pump 10. Once a new pump 10 is placed in the pump cradle 412 and the pump drawer 402 is closed and locked, as described in the foregoing, the piston linear actuators 462 associated with the two (2) outer slide blocks 470 may be driven so that the slide blocks 470 move distally or forward in their slide block apertures 518 and enabling the clamping block 522 to compressively engage the rear or proximal side of the front plate 102 of the pump body 100 of the replacement pump 10.

[00222] The pump clamping section or mechanism 520 further comprises a pressure measurement mechanism 552 for interfacing with the outlet selector valve 280 and, in particular, the rear or proximal pressure sensing port 296 defined in the outlet selector valve cylinder 264 on the manifold plate 230. The pressure measurement mechanism 552 comprises a hollow support block or housing 554 seated on a top face of the clamping block 522. The support block or housing 554 defines an interior chamber 556 that supports a pressure sensor interface pin 558 and a pressure measurement load cell 560 operatively engaged with the pressure sensor interface pin 558. The support block or housing 554 comprises a front or distal end 562 defining a cylindrical front or distal port 564 defining a through bore through which the pressure sensor interface pin 558 projects so as to extend outward from the front port 564 to contact the pressure sensing diaphragm 298 in the rear or proximal pressure sensing port 296 in the outlet selector valve cylinder 264 on the manifold plate 230. The distal end 562 of the support block 554 is in contact or seats against the top lip or flange 538 on the clamping block 522. The front port 564 is adapted to engage the rear or

proximal pressure sensing port 296. The pressure measurement load cell 560 is in operative engagement with the pressure sensor interface pin 558 so that fluid pressure changes as exerted on the pressure sensing diaphragm 298 in the rear or proximal pressure sensing port 296, which reflects the fluid pressure changes in the outlet manifold channel 244, are transmitted to the pressure measurement load cell 560. The pressure measurement load cell 560 converts movement of the pressure sensing diaphragm 298 into an electronic signal that is transmitted to the sensor control board 804 via an electronic link or connection 566. The sensor control board 804 continuously relays this pressure information to the control system 800 so that fluid pressure within the outlet manifold channel 244 may be measured and tracked. This measurement enables the control system 800 to ascertain the fluid pressure in the patient outlet port 270 or the waste outlet port 272 depending on the rotational position of the outlet selector valve 280.

The pressure measurement load cell 560 is preloaded by a preload spring 568 [00223] which is supported at one end on a spring guide 570 extending rearward or proximally from the rear side of the support block or housing 554, and has a second end secured to a spring support 572 secured to the two (2) rearmost (e.g., proximal) support appendages 534 extending upward from the clamping block 522. A cover 574 may be provided to enclose the interior chamber 556 in the support block 554. The support block 554 may be secured against upward movement in the proximally extending slot 512 in the top support plate 424 by a suitable restricting connection with the opposed ledges 514 along the walls of the proximal slot 512 or suitable connection with the clamping block 522 itself. The preload spring 568 provides sufficient preloading to the pressure measurement load cell 560 and further ensures that the front port 564 on the front or distal end 562 of the support block 554 remains operatively seated or engaged in the rear or proximal pressure sensing port 296 in the outlet selector valve cylinder 264 on the manifold plate 230 when the pump 10 is in operation and under pressure. The operative engagement between the front port 564 and the pressure sensing port 296 maintains operative contact or interface between the pressure sensor interface pin 558, which projects outward or distally from the front port 564, and the pressure sensing diaphragm 298 in the pressure sensing port 296 in the outlet selector valve cylinder **264**. Although many pressure sensing devices are available that use a diaphragm and load cell to measure pressure, in the present embodiment, since the pressure sensing diaphragm 298 is located in the disposable pump 10 and the pressure measurement load cell 560 and pressure sensor interface pin 558 are located in the reusable drive and actuating system 400, a more robust and sensitive load cell may be used for the pressure measurement load cell 560. This

arrangement allows the fluid-contacting diaphragm **298** to be replaced frequently for sterility purposes, while permitting the use of a high-precision load cell for the pressure measurement load cell **560**.

[00224] From the foregoing, it will be understood that the clamp actuating mechanism **540**, which retracts the clamping block 522 from compressive engagement with the front plate 102 of the pump body 100, as described in the foregoing, also affects operation of the foregoing pressure measurement mechanism 552. For example, if a pump 10 is loaded in the pump cradle 412 in the pump drawer 402 and it is desired to remove the existing pump 10, the piston linear actuators 462 associated with the two (2) outer or outboard slide blocks 470 may be operated so that the slide blocks 470 move proximally or rearward in their respective slide block apertures 518 toward the rear support plate 422, which concurrently moves the clamping block 522 proximally or rearward via the clamp actuating mechanism 540 as discussed in the foregoing. This movement disengages the clamping block 522 from contact with the front plate 102 of the pump body 100 of the pump 10. As the support block 554 is supported by the clamping block 522, forward or rearward movement of the clamping block 522 likewise moves the pressure measurement mechanism 552 in its entirety. Accordingly, as the clamp actuating mechanism 540 retracts the clamping block 522 in the manner described previously, the pressure measurement mechanism 552 is likewise retracted and the front port 564 on the front or distal end 562 of the support block 554 is likewise disengaged from the rear or proximal pressure sensing port 296 in the outlet selector valve cylinder 264 on the manifold plate 230, and the pressure sensor interface pin 558 is removed from operative contact with the pressure sensing diaphragm 298 in the pressure sensing port 296. Upon loading of a new pump 10 in the pump drawer 402, the piston linear actuators 462 associated with the two (2) outer or outboard slide blocks 470 may be driven so that the slide blocks 470 move distally or forward in their respective slide block apertures 518 and enable the clamping block 522 to compressively engage the rear or proximal side of the front plate 102 of the pump body 100 of the replacement pump 10. This distal or forward movement of the clamping block 522 likewise places the front port 564 on the front or distal end 562 of the support block 554 in engagement with the rear or proximal pressure sensing port 296 in the outlet selector valve cylinder 264 on the manifold plate 230, and the pressure sensor interface pin 558 is placed in operative contact or engagement with the pressure sensing diaphragm 298 in the pressure sensing port 296 in the outlet selector valve cylinder 264. As noted previously, the preload spring 568 provides sufficient preloading to the pressure measurement load cell 560 and further ensures that the front port 564 on the front or distal end 562 of the

support block **554** remains operatively seated or engaged in the rear or proximal pressure sensing port **296** in the outlet selector valve cylinder **264** on the manifold plate **230** when the pump **10** is in operation and under pressure.

[00225] In operation, fluid pressure transmitted through the pressure sensing diaphragm 298 applies a representative force to the pressure measurement load cell 560, which converts the pressure-dependent force to an electronic signal that can be used by the control system 800. The force applied to the pressure sensor interface pin 558 is substantially proportional to the fluid pressure and the cross-sectional area of the pressure sensing diaphragm 298. Since the cross-sectional area of the pressure sensing diaphragm 298 remains substantially constant, the output of the pressure measurement load cell 560 is generally proportional to the fluid pressure. Features may be provided between the front port 564 on the front or distal end 562 of the support block 554 and the rear or proximal pressure sensing port 296 in the outlet selector valve cylinder 264 to ensure proper alignment between the pressure measurement load cell 560 and the disposable pump 10. The elastomeric pressure sensing diaphragm 298 is desirably formed during a secondary molding operation that occurs after the manifold plate 230 is molded.

The outlet selector valve actuating section 580 is disposed on top of the top [00226] support plate 424 that supports the various components of the outlet selector valve actuating section 580. The outlet selector valve actuating section 580 provides the drive and mechanical interfacing components for operating the outlet selector valve 280. The outlet selector valve actuating section 580 comprises a support platform 582 disposed and supported on the top side of the top support plate 424. The support platform 582 extends across the proximal slot 512 in the top support plate 424. The outlet selector valve actuating section 580 further comprises an outlet selector valve actuator 584 driven by an outlet selector valve drive motor 600. The outlet selector valve actuator 584 comprises an actuator element 586 comprising an upper or top end 588 and a lower or bottom end 590. The top end 588 of the actuator element 586 is rotationally supported by suitable rotational support bearings 592 in an actuator enclosure housing 594 supported on the support platform 582. The rotational support bearing 592 in the actuator enclosure 594 vertically and rotationally supports the upper or top end 588 of the actuator element 586. An electro-mechanical angular position sensor 596, such as a rotary encoder, is mechanically coupled to the upper or top end 588 of the actuator element 586. The angular position sensor 596 is electronically linked to the control system 800 via an electronic link or connection 598 to the sensor control board 804. The angular position sensor 596 is operable to determine the specific angular orientation of

the valve stem **286** of the outlet selector valve body **282** of the outlet selector valve **280**, which is relayed to the control system **800** via the sensor control board **804**. From the foregoing, it will be understood that the control system **800** receives signal information from the angular position sensor **596** associated with the actuator element **586** and may operate the drive motor **600** to set the angular orientation of the valve stem **286** of the outlet selector valve body **282** of the outlet selector valve **280** in any one of the operating states discussed previously, or any desired angular position in the outlet selector valve cylinder **264** on the manifold plate **230**.

The outlet selector valve drive motor **600** is likewise supported by the support platform 582 adjacent the outlet sector valve actuator 584. The outlet selector valve drive motor 600 has an output drive shaft 602 that extends through the support platform 582. A drive pulley 604 is mounted on the drive shaft 602 below the support platform 582 and an actuator pulley 606 is mounted to the lower or bottom end 590 of the actuator element 586. A timing belt 608 is reeved about the drive pulley 604 on the drive shaft 602 and the actuator pulley 604 mounted to the lower or bottom end 590 of the actuator element 586 to rotationally interface the drive shaft 602 and the actuator element 586 so that rotation of the drive shaft 602 imparts corresponding rotary motion to the actuator element 586. The outlet selector valve drive motor 600 may be a servomotor or stepper motor that is electronically linked to the sensor control board 804 via an electronic link or connection 610 so that the control system 800 may control operation of the drive motor 600 and, hence, control operation of the outlet selector valve actuator 584. The sensor control board 804 provides power to the drive motor 600 via the electronic link or connection 610. Accordingly, by controlled operation of the outlet selector valve drive motor 600, the outlet selector valve 280 may be angularly positioned to one of the desired operating positions discussed previously, or any desired angular position, and the angular position of the valve stem 286 of the outlet selector valve 280 is monitored by the angular position sensor 596 coupled to the top end 588 of the actuator element 586 and linked to the control system 800 via the sensor control board **804**.

[00228] The lower or bottom end 590 of the actuator element 586 is formed with an actuator head 612 that defines a U-shaped pocket 614 for receiving the actuator interface head 284 at the top end of the valve stem 286 of the outlet selector valve body 282 of the outlet selector valve 280. As noted previously, the actuator interface head 284 is generally T-shaped and comprises two (2) outwardly extending tabs 292. The U-shaped pocket 614 accommodates the T-shaped interface head 284 with the outward extending tabs 292 seating

against the face of the actuator head 612. The T-shape of the actuator interface head 284 allows the outlet selector valve body 282 to slide into engagement with the pocket 614 in the actuator head 612 and "keys" the outlet selector valve body 282 so that it may be engaged by the actuator head 612 in only one particular orientation. The interface between the actuator interface head 284 and the actuator head 612 also prevents the outlet selector valve body 282 from being ejected upward from the outlet selector valve cylinder 264 on the manifold plate 230 under high pressure as the actuator element 586 is limited in the vertical direction by the rotation support bearings 592 in the actuator enclosure 594. The actuator element 586 is desirably vertically positioned above the clamping block 522 and the pressure measurement mechanism 552 so that when the pump 10 is loaded into the pump cradle 412 in the pump drawer 402, the actuator interface head 284 at the top end of the valve stem 286 of the outlet selector valve body 282 of the outlet selector valve 280 is diametrically opposed to the U-shaped pocket 614 in the actuator head 612. Accordingly, as the pump drawer 402 is closed, the U-shaped pocket 614 automatically receives the T-shaped actuator interface head 284.

[00229] A main power supply coupling 620 may be mounted on the base plate 432 and the rear support plate 422. The power supply coupling 620 provides power to the drive control board 802 and the sensor control board 804, and suitable power supply cabling 622 from the drive control board 802 provides power to the various piston drive motors 442 and inlet selector valve drive motors 444 in the drive section 440. The base plate 432 includes an electronic connection port 624 for electronically connecting the drive control board 802 to the control system 800. The sensor control board 804 may likewise be electronically connected to the electronic connection port 624 for electronically connecting the sensor control board 804 to the control system 800.

[00230] A power and signal coupling 620 may be connected to the drive control board 802 and the sensor control board 804. The power and signal coupling 620 provides power to the sensor control board 804, and transfers control signals between the drive control board 802 and the sensor control board 804. Suitable power supply cabling 622 from the drive control board 802 provides power to the various piston drive motors 442 and inlet selector valve drive motors 444 in the drive section 440. The drive control board 802 may include an electronic connection port 624 for electronically connecting the drive control board 802 to the control system 800. The sensor control board 804 may likewise be electronically connected to the control system 800 via the power and signal coupling 620 and electronic connection port 624. The drive control board 802 is supported by the base plate 432 extending rearward from the rear support plate 422.

[00231] As noted in the foregoing, the drive and actuating system 400 and, desirably, the control system 800 are supported and contained by the mobile support 700. The mobile support 700 generally comprises a support housing 702 vertically supported by a support pedestal or column 704 connected to a wheeled base 706. The wheeled base 706 permits the mobile support 700 to be movable within a hospital or like medical facility. The pedestal 704 may include a handle structure 708 for moving the mobile support 700. Bottle or container supports 710 may be provided on lateral sides of the pedestal 704 for stably supporting bottles or containers, such as the fluid source containers 30 discussed previously, during spiking operations. The bottle or container supports 710 allow bottles or containers to be spiked and to be maintained in an upright posture during spiking at a location near the pump drawer 402 since the fluid supply tubes 34 of the various embodiments of the fluid supply sets 32 are typically permanently affixed to the pump 10. Additionally, the support housing 702 may comprise two (2) lateral fluid handling compartments 712, as shown in FIG. 60, which are supported within respective lateral compartment doors 714 that close against and form part of the support housing 702 of the mobile support 700. These lateral fluid handling compartments 712 house components of the fluid management system 720 and, thus, the lateral fluid handling compartments 712 support and maintain the various diagnostic or therapeutic (e.g., pharmaceutical) fluids to be associated with the pump 10. The mobile support 700 also supports components of the control system 800, as shown in FIG. 46A. While the details of the control system 800 are provided herein, FIG. 46A shows certain components of the control system 800 supported on the support housing 702 including a local user interface display 806, typically a touch screen, a packaging reader 808 such as bar code or RFID tag reader, and a patient outlet air detector 810 which interfaces with and accepts the medical tubing of the patient supply set 40. A patient outlet port opening 716 is further provided in the support housing 702 to provide an egress opening for the swabable valve 274 seated in the patient outlet port 270 on the outlet selector valve cylinder 264 on the manifold plate 230. Further, the handle housing portion 404 and waste collection compartment 406 of the pump drawer 402 are accessible from the front of the support housing 702 and are formed to blend cosmetically as part of the support housing 702. If desired, the support housing 702 may be detachable from the pedestal 704 and may include overhead mounting points 718 on a top or upper face for mounting the support housing 702 to an overhead support system (not shown). The support housing 702 and support pedestal 704 together may have any suitable ornamental appearance.

[00232] As shown in FIG. 60, each fluid handling compartment 712 encloses a fluid management system 720. In particular, the fluid management system 720 comprises identical fluid handling arrangements, one in each fluid handling compartment 712. Each fluid handling arrangement comprises a saline container support or hanger 724 supporting a saline fluid source container 30 such as a saline bag, and a pair of fluid container supports 726 for supporting one of the fluid source containers 30, discussed previously, in an inverted fluid delivery orientation. Any type of support or hanger may be provided for supports or hangers 724, 726, such as those described in U.S. Patent No. 7,240,882 to Degentesh, et al. incorporated herein by reference for this purpose.

[00233] Upper and lower indicator lights 728, 730 are provided in the interior of the fluid handling compartment 712, above and below each of the saline container support 724 and the respective fluid container supports 726. The upper and lower indicator lights 728, 730 may be controlled by the control system 800 to alert the operator via visual means (and potentially augmented by auditory or other means) as to the location in the respective fluid handling compartments 712 where the fluid source containers 30 should be placed for an injection procedure. The indicator lights 728, 730 may be color coded to correspond to a specific fluid. For example, the indicator lights 728, 730 associated with the saline support 724 may be blue, while the indicator lights 728, 730 for the fluid container supports 726 in the left fluid handling compartment 712 are green, and the indicator lights 728, 730 for the fluid container supports 726 in the right fluid handling compartment 712 are purple, as examples. Additionally, a pump connection status bar 732 is provided in the interior of each of the fluid handling compartments 712 in a lower corner and contains three (3) indicator lights, designated as 732a, 732b, 732c in FIG. 60. These indicator lights 732a, 732b, 732c correspond, respectively, to the three (3) pairs of indicator lights 728, 730 and, ideally, have the same color-coding as the corresponding indicator lights 728, 730. Accordingly, indicator light 732a may be blue to correspond to the indicator lights 728, 730 associated with the saline support 724, and indicator light 732b may be green to correspond to the indicator lights 728, 730 associated with the "center" or "middle" fluid container supports 726 in the left fluid handling compartment **712**, etc.

[00234] As described in detail herein, when a new fluid source container 30 is installed in a fluid handling compartment 712, the control system 800 causes all three (3) indicator lights 728, 730, 732 for that source location to flash or blink together. The indicator lights 728, 730 respectively show the user where to place the fluid source container 30 and which associated air detector (as described herein) is active for that fluid source container 30. The lower

indicator light **730** also shows the user which of the three (3) fluid supply tubes **34** on that side of the pump **10** should be used to connect to the fluid source container **30**. Once the fluid source container **30** is installed and successfully primed, all three indicator lights **728**, **730**, **732** change from flashing or blinking to solid "on". This indicates that the fluid source container **30** is "active" and available for use if desired. Once the fluid source container **30** has been depleted, the control system **800** turns all three (3) indicator lights **728**, **730**, **732** "off" to show that the fluid source container **30** is no longer available. If the "open life" of the fluid source container **30** expires or if the user indicates that the fluid source container **30** should no longer be used, the indicator lights **728**, **730**, **732** are turned "off". The indicator lights **728**, **730**, **732** are not typically used during a fluid injection as they are typically closed behind the lateral compartment doors **714** during fluid injections.

[00235] As was described previously, each pump 10 in the illustrated embodiment comprises a pump body 100 with three (3) inlet ports 122, 124, 126 on each lateral side, including two (2) fluid inlet ports 122, 124 and a single saline inlet port 126. To accommodate this embodiment of the pump 10, each fluid handling compartment 712 is adapted to support three (3) fluid containers 30 to be associated with the inlet ports 122-126 on the lateral sides of the pump body 100. However, this configuration of the pump 10, as noted previously, is merely exemplary and should not be considered limiting. The pump 10 and the foregoing corresponding configuration of the respective fluid handling compartments 712 should not be considered as exclusive and the pump 10 and the respective fluid handling compartments 712 may be expanded to include additional fluids (e.g., four (4) or more fluids), or fewer fluids (e.g., less than three (3) fluids). However, the arrangement of two (2) fluid handling compartments 712, each supporting up to three (3) fluid source containers 30, is desirably effective for interfacing with the pump 10.

[00236] The respective fluid handling compartments 712 also each support a series of fluid inlet air detectors 812, 814, 816 for the fluid supply tubes 34 used to conduct fluids from the respective fluid source containers 30. The inlet air detectors are respectively associated with the saline container support 724 and the respective fluid container supports 726 in the fluid handling compartments 712. The air detectors 812-816 and the patient outlet air detector 810, discussed previously, provide air bubble detection information to the control system 800 for operational control of the fluid delivery system 2. The various air detectors 810-816 may be conventional optical or ultrasonic air detectors as are well known in the medical field, and are discussed further herein.

[00237] Further, it is often desirable to maintain the fluid contained in the various fluid source containers 30 in each fluid handling compartment 712 in a warmed state for the comfort of the patient and other purposes. For example, in the case of contrast media used in radiographic imaging procedures, increasing the temperature of the contrast media also has the desirable effect of reducing the viscosity of the contrast media for easier injection into the patient, among other advantages. Accordingly, each fluid handling compartment 712 is warmed by a convective heating system 734. The convective heating system 734 may include devices or components (not shown) that may intake air through an intake vent 736 in each fluid handling compartment 712, warm the air across a heating system, such as simple electrical resistance coils, and return the heated air into the interior of the fluid handling compartment 712 via an air outlet vent 738.

[00238] During a fluid injection, one or more indicator lights 807 on the user interface display 806 may be turned on by the control system 800 to show which fluids are being injected. For example, the indicator lights 807 may be two (2) multi-color indicator lights located in the top left and right corners of the user interface display 806. The indicator lights 807 may be either flashing or solid "on" and may emit white, blue, green, purple, etc. light depending on the fluid being injected. For example, if saline is being injected into the patient, the indicator lights 807 may be blue based on the color convention discussed previously in connection with the indicator lights 728, 730, 732 in the fluid handling compartments 712. Both indicator lights 807 desirably always display the same state (flashing or solid "on" and the same color). Additional and larger indicator lights (not shown) may be placed on the user interface display 806 or on the support housing 702 and may be sized so that a user is able to see these indicator lights from anywhere in the room where the fluid delivery system 2 is located. These "larger" indicator lights (not shown) desirably indicate when the fluid delivery system 2 is armed and during a fluid injection, and may show which type of fluid is currently being injected. For example, if saline is being injected, these larger indicator lights can flash blue, and if contrast from the left fluid handing compartment 712 is being injected, the larger indicator lights can flash green.

[00239] Turning next to operational aspects of the fluid delivery system 2, it will be understood that numerous steps are undertaken during "normal" or "typical" setup and operation of the system 2. The following discussion outlines a series of steps that typically occur during normal setup and operation of the fluid delivery system 2. The following operational discussion is intended as exemplary and non-limiting, and generally outlines the steps and procedures for normal or typical setup and operation from which one skilled in the

art may operate the fluid delivery system 2. Operation of the fluid delivery system 2 may be considered to be divided into a number of different procedures or steps such as installing a pump 10, priming the pump 10 and associated inlet fluid handling components, priming the outlet patient supply set 40, etc. Relevant procedures and steps are described hereinafter for installing a pump 10, priming the pump 10 and associated inlet fluid handling components, and priming the outlet patient supply set 40. Reference continues to FIGS. 1-60 hereinafter. Initially, the control system **800** of the fluid delivery system **2** is turned "ON" and provided with power, which boots up all processors, sensors, such as the angular position sensors 494, 596, drawer closed sensor 818, and drawer locked sensor 820, as examples, and the user interface display 806. The foregoing listing is not intended to be exhaustive. It will be appreciated that the control system 800 comprises a system controller or computer 822 with appropriate software for controlling operation of the fluid delivery system 2 and this controlling computer may physically reside on-board the mobile support 700, or be located at some external location, such as in a control room, and interface via a hardwired connection or wireless connection, as desired, with the electronic components associated with the support housing 702, such as the drive control board 802 and sensor control board 804, sensors, such as the angular position sensors 494, 596, drawer closed sensor 818, and drawer locked sensor 820, as examples, and the user interface display 806. While the microprocessor and like components for controlling the various components of the drive and actuating system 400 may reside entirely with the system controller 822, these control components may be distributed between the system control computer 822 and the drive control board 802 and sensor control board 804 as desired by one skilled in the computer field. The system controller 822 may interface via wired or wireless connections with external devices such as a computer network 900 (via an Ethernet connection), a CT scanner 902, a remotely located display 904, such as a touch screen, and like external devices, as shown in FIG. 46B. Further, it will be appreciated by one skilled in the computer field that all of the processing, data storage, and other computer-implemented tasks described herein may be performed by the control system 800, the system controller 822 or any other device with such capabilities that is in communication with the control system 800 and/or the system controller 822. Such a device may be in communication with the control system 800 and system controller 822 via a computer network 900 or any other means for wired or wireless data communication.

[00241] Safety tests and internal self tests are performed on various parts of the control system 800, such as the air detectors 812-816, the optical sensor or like detector (not shown) used to read the pump indicator plate 170, and the user interface display 806, and other

various sensors physically included in the drive and actuating system 400, such as the drawer closed sensor 818, drawer locked sensor 820, angular position sensors 494, 596, pressure measurement mechanism 552 (e.g., strain gauge/load cell 560), etc. The control system 800 includes an optical sensor or like detector (not shown) associated with the drive and actuating system 400 used to read the pump indicator plate 170 to confirm that no pump 10 is currently installed in the pump drawer 402. If the control system 800 is recovering from a power failure or other unusual event and a pump 10 is already associated with the drive and actuating system 400, a more complex recovery sequence may be executed by the system controller 822. The piston drive motors 442 for the four (4) piston linear actuators 462 are "homed" by moving them until a "home sensor" 824 for each actuator 462 is tripped thereby resetting their positions to zero. Each home sensor 824 is electronically connected with the sensor control board 804 as best shown in FIGS. 54 and 58. The inlet selector valve drive motors 444 for the respective inlet selector valve actuators 464 and the outlet selector valve drive motor 600 for the outlet selector valve actuator 584 are moved to their "home" positions by using the angular position sensors 494, 596 associated with each actuator 464, **584**. It is now possible for a user to begin using the fluid delivery system 2.

Before an injection procedure may be performed, several setup steps are typically [00242] required including, but not limited to: (1) installing a pump 10 and priming the same with saline S1, S2; (2) installing the fluid source containers 30 having sufficient volume of saline S1, S2 and therapeutic or diagnostic (e.g., pharmaceutical) fluids A1, A2 and B1, B2, to support the desired patient protocol, which also may be termed a fluid injection procedure; (3) installing a patient supply set 40 to the pump 10 and priming the same with saline S1, S2; (4) programming a patient protocol or selecting a patient protocol from protocol storage in the system controller 822 and which is accepted by the control system 800 as "valid"; and (5) assuring that there is sufficient free space in the waste collection container 48 to accept any waste fluid that may be generated during the fluid injection procedure. It will be understood that the foregoing steps do not have to be performed in the order listed, but some steps may depend on the successful completion of a previous step. For example, it is possible for the user to enter a patient protocol first and then subsequently install the fluid source containers 30 but it is not possible to install the fluid source containers 30 or attach a patient supply set 40 until the pump 10 is installed in association with the drive and actuating system 400. The foregoing steps are described in greater detail herein.

[00243] Initially, it is desirable to install a pump 10 in association with the drive and actuating system 400. The user interface display 806 typically displays a "Home Screen".

The user first opens the packaging containing a pump 10 and removes the pump 10 from the packaging. The user scans or otherwise reads the identifying indicia 172, such as a bar code or RFID tag, using the packaging reader 808 on the mobile support 700. As an alternative, the user may use the user interface display 806 to indicate that a new pump 10 is being installed and can manually enter the barcode digits and like information read from the identifying indicia 172. If the packaging reader 808 is equipped to read an RFID tag, the information contained thereby may be read by the packaging reader 808. An RFID tag reader may also, or alternatively, be present within the drive and actuating system 400 so that the RFID tag as the identifying indicia 172 may be "read" when the pump 10 is installed in the drive and actuating system 400. In this situation, the pump 10 is installed in the pump drawer 402, and when the pump drawer 402 is closed and locked the RFID tag reader "reads" the information container in the RFID tag identifying indicia 172 and may further "write" to the RFID tag identifying indicia 172, as discussed previously. The foregoing "internal" RFID tag reader may take the place of the optical sensor or like detector (not shown) used to read the pump indicator plate 170.

The control system 800 now automatically switches the user interface display 806 [00244] to a "Pump Installation Dialog Screen". The system controller 822 decodes the information contained in the identifying indicia 172 from the packaging reader 808 and indentifies one or more of the: pump type/configuration, pump serial number, pump manufacturing identification number, use-by date, manufacturing lot code/batch number, and initial angular position (e.g., inlet selector valve position code) of the inlet selector valves 300. The system controller 822 desirably checks the pump serial number against an internal database. If the pump serial number is already in an internal database of "used pumps", the control system 800 generates a message on the user interface display 806 to indicate that pump 10 cannot be used. The control system 800 uses the inlet selector valve position code to determine the initial angular position of the inlet selector valves 300 which informs the system controller 822 as to the initial or "preset" angular orientation of the valve stem 306 of the inlet selector valve body 302 and, hence, the initial angular positions of the inlet ports 322-328 in the valve stem 306. From the initial angular orientation of the valve stem 306 of the inlet selector valve body 302 for the respective inlet selector valves 300, the system controller 822 positions the respective inlet selector valve actuators 464 to correctly match the angular orientation of the inlet selector valves 300. The outlet selector valve actuator 584 operates the outlet selector valve 280 to place the outlet selector valve body 282 in a "waste" position in which the flow passage 290 in the outlet selector valve body 282 of the outlet selector valve 280 is placed in

fluid communication with the waste outlet port 272 on the outlet selector valve cylinder 264 on the manifold plate 230. The piston drive motors 442 for the four (4) piston linear actuators 462 move the respective piston linear actuators 462 to their fully retracted (rearmost) position. The piston linear actuators 462 generally operate behind the normal working or pumping zone 164 of the pump cylinders 104 before the plungers 200 are connected thereto and then may operate in the normal working or pumping zone 164 of the pump cylinders 104 after the plungers 200 are connected thereto. The retraction of the two (2) outboard piston linear actuators 462 compresses the clamping springs 532 and withdraws the clamping block 522 to permit pump installation, in the manner described previously hereinabove.

[00245] As noted in the foregoing, retraction of one of the inboard piston linear actuators 462, namely the left inboard piston linear actuator 462 in the description provided in the foregoing, moves a lock actuator (not shown), such as a cam mechanism, to move the locking support plate 416 to the unlocked position, which unlocks the pump drawer 402. The user then opens the pump drawer 402 in the front of support housing 702, inserts the pump 10 into pump drawer 402, and places it in the pump cradle 412. The attached waste collection system 44 is placed in the waste collection compartment 406. The user then closes the pump drawer 402. Once closed, the control system 800 desirably locks the pump drawer 402. The control system 800 detects that the pump drawer 402 is closed via the drawer closed sensor 818 and operates the drive motor 442 associated with the left inboard piston linear actuator 462 to move the left inboard piston linear actuator 462 slightly forward to actuate the lock actuator to move the locking support plate 416 to the locked position. The control system 800 confirms that the pump drawer 402 has been locked with the drawer locked sensor 820.

[00246] The control system 800 then operates the drive motors 442 for the two (2) outboard piston linear actuators 462 to move these actuators forward slightly to release the clamping springs 532, permitting the clamping block 522 to apply a compressive force to the rear of the front plate 102 of the pump body 100 and clamp the pump 10 in place in the pump cradle 412. When the clamping springs 532 apply compressive force to the pump 10, the pressure measurement mechanism 552 is automatically engaged with the pressure sensing diaphragm 298 in the pressure sensing port 296 in the outlet selector valve cylinder 264 on the manifold plate 230, and the optical sensor or detector (not shown) used to read the pump indicator plate 170 on the pump body 100 also engages or interfaces with the pump 10. The control system 800 uses the optical sensor or detector (not shown) to read the groove pattern of the pump indicator plate 170 and confirms that this pattern matches at least the pump type encoded in the barcode or RFID tag forming the identifying indicia 172. The strain

gauge/load cell **560** of the pressure measurement mechanism **552** is "zeroed", meaning that the current sensor value is recorded as a zero pressure value.

Additionally, all four (4) piston linear actuators 462 are "calibrated" to the pump 10. In this calibration step, the pistons 50 are advanced to contact the rear face of their respective plungers 200. The piston linear actuators 462 push the plungers 200 from the rear "assembly" or isolation zone 166 into the forward "working" or "pumping" zone 164 of the respective pump cylinders 104. The piston linear actuators 462 continue to push the plungers 200 into the pump chambers 106 of the pump cylinders 104. As the front or distal end disc 206 on each plunger 200 contacts the distal end 108 of the pump cylinder 104 formed by the front plate 102 of the pump body 100, the respective pistons 50 "snap" onto the respective plungers 200 via the snap-fit connection described previously. At this point, the electrical current in the associated drive motor 442 will increase significantly (e.g., "spike"). The control system 800 detects each current "spike" via the respective electronic connections 450 between the drive motors 442 and the drive control board 802. The control system 800 stops the respective drive motors 442, moves the piston linear actuators 462 rearward slightly, and then sets a "zero volume position" for each pump cylinder 104. The left and right inlet selector valves 300 are moved to their "OFF" positions. The user may open the lateral compartment doors 714 at this time, or these doors 714 may be opened earlier in the foregoing process. Saline fluid source containers 30 may be installed in the lateral fluid handling compartments 712 and the saline priming process may now begin. The foregoing presupposes that the pump drawer 402 is locked and the pump 10 is held in place by the clamp actuating mechanism **540**.

[00248] The user typically scans a barcode and like indicia on the saline fluid source container/bag 30 using the packaging reader 808 on the mobile support 700. Alternatively, the user may use the user interface display 806 to manually indicate that a new saline fluid source container 30 is being installed and specify the type and container size. The control system 800 identifies the type and size of the saline source S1 that is being installed and displays the information on the user interface display 806. The control system 800 indicates on the user interface display 806 that the saline fluid source container 30 is to be installed in the left side fluid handling compartment 712, as viewed from the front of the mobile support 700 (e.g., the view of FIG. 60) so that the left side of the pump 10 is supplied by the first saline fluid source container 30. The control system 800 causes the upper and lower indicator lights 728, 730 associated with the saline support 724 in the left fluid handling compartment 712 to flash, blink, or otherwise visually indicate to the user as to where the saline fluid

source container 30 should be installed. An additional lower indicator light 730 may be provided adjacent the rearmost saline air detector 816 and can flash, blink, or otherwise visually indicate that this rearmost saline air detector 816 is used for the fluid supply tube 34 connected to the spike 36 used to access the saline fluid source container 30. Depending on the configuration of the fluid supply set 32 provided with the pump 10, as shown in FIGS. 40-43 discussed previously, the user may be required to clean a swabable valve 70 associated with the fluid supply tube 34 and connect a spike 36 thereto to access the saline fluid source container 30. However, the relevant point is that the rearmost fluid supply tube 34 associated with the rearmost saline inlet port 126 on the left side 18 of the pump body 100 of the pump 10 is connected to the first saline fluid source container 30 that is loaded into the left fluid handling compartment 712. The user also inserts the fluid supply tube 34 into the air detector 816, and the flashing lower indicator light 730 near the air detector 816 guides the user in associating the fluid supply tube 34 with the correct "saline" air detector 816. The control system 800 detects that the fluid supply tube 34 is installed in the air detector 816 and enables a "Prime" button on the user interface display 806 which may be disabled or "grayed out" prior to the foregoing installation of the fluid supply tube 34 with the air detector 816.

The user may then press the "Prime" button and the fluid supply tube 34, inlet [00249] selector valves 300, and inlet manifold channels 236 are primed with saline. The outlet selector valve 280 is rotated to the waste position (if not already in position), as described previously, and the left and right inlet selector valves 300 are moved from the "OFF" position to a "left saline source" or "S1" position to allow fluid communication between the rear saline channel 134 of the saline manifold 130 and the rearmost saline port 334 in the valve stem 306 of the inlet selector valve body 302 of both inlet selector valves 300. All four (4) plungers 200 are retracted substantially simultaneously to pull air/saline from the left saline fluid source container 30 into the rear saline channel 134 of the saline manifold 130 via the left saline inlet port 126 on the left side inlet selector valve cylinder 114 of the pump body 100. The plungers 200 are retracted to deliver up to a predetermined or preset priming volume of air/saline into the pump chambers 106. The pump cylinders 104 on the left side 18 of the pump body 100 draw air/saline from the left saline fluid source container 30, through the fluid supply tube 34, through the left inlet selector valve 300 and left inlet manifold channel 236, and into the two (2) left pump cylinders 104. The pump cylinders 104 on the right side 16 of the pump 10 draw air/saline from the left saline fluid source container 30, through the fluid supply tube 34, across the rear saline channel 134, through the right inlet selector valve 300 and right inlet manifold channel 236, and into the two (2) right pump

cylinders **104**. At this point all four (4) pump cylinders **104** contain a mixture of air and saline. All four (4) plungers **200** are then advanced substantially simultaneously to eject the air/saline mixture into the waste collection container **48**. As this mixture is ejected, the pressure sensor output signal from the pressure measurement mechanism **552** is monitored. If the pressure exceeds a predetermined limit, indicating a blockage in the waste collection tube set **46**, the priming process is halted.

If, in the foregoing process, the final extracted volume (X ml) of air and saline from the left saline fluid source container 30 contains less than a predetermined volume of air (Y ml), as determined by the system controller 822 based on sensed air detection information from the left saline air detector 816, priming of the fluid supply tube 34 is considered complete (e.g., X>Y). If more than a predetermined maximum volume of air (Y ml) was determined by the system controller 822 based on sensed air detection information from the left saline air detector 816, the user is prompted via the user interface display 806 to repeat the foregoing priming process. The control system 800 may also query the user via the user interface display 806 to visually confirm that the fluid supply tube 34 is free of air and that the priming process is complete. If the user sees air in the fluid supply tube 34, the user may initiate a repeat of the priming process using the user interface display 806. In other words, in this saline priming process, a predetermined volume of air and saline (X ml) is extracted from the left saline source container 30 and at least a minimum volume (e.g., X ml - Y ml) has to be free of air to consider this priming process complete. The system controller 822 is programmed in advance with information (X ml and Y ml) that a certain minimum or predetermined volume of saline must be drawn from the left saline fluid source container 30 in order to prime the downstream volume of the fluid supply tube 34, inlet selector valves 300, and inlet manifold channels 236, and can cause the drive pistons 50 to withdraw the plungers 200 a predetermined distance or "stroke" in the pump cylinders 104 to ensure that the predetermined minimum volume of saline is present for the priming of the fluid supply tube 34. If for any reason the left saline air detector 816 registers the presence of air after the forward or priming stroke of the respective pistons 50, the system controller 822 will require a repeat of the foregoing priming process.

[00251] The control system 800 also initiates clearing or purging of air from the outlet manifold channel 244. In this procedure, all four (4) plungers 200 are retracted substantially simultaneously to pull fluid from the left saline fluid source container 30 into the pump 10 up to a predetermined flushing volume. All four (4) plungers 200 are then advanced to eject the saline in the pump cylinders 104 into the waste collection container 48, clearing the outlet

manifold channel 244 of air in the process. The pump 10 and the fluid path including the fluid supply tube 34 to the left saline fluid source container 30 are now primed with saline and the control system 800 records the installation time of the left saline fluid source container 30. This recorded information may be displayed for the user on the user interface display 806 or may be automatically or manually viewed at a later point in time, if desired. The control system 800 may also provide and initialize a countdown timer that may be viewed at any time on the user interface display 806 to see the remaining "open life" of the saline in the left saline fluid source container 30 based on manufacturer's information and/or other guidelines for the permitted "open life" of the fluid. The control system 800 also may display expiration warnings on the user interface display 806 when there is less than a predetermined amount of remaining "open life" and when the remaining "open life" has reached zero. Further, the control system 800 moves the inlet selector valves 300 to their "OFF" positions and moves the outlet selector valve 280 to the "OFF" position. The control system 800 then changes the indicator lights 728, 730 associated with the left saline fluid source container 30 and the saline air detector 816 from flashing to solid, as an example, to indicate that the fluid source container 30 has been installed, primed, and ready for use. If desired, the control system 800 may now prime the patient supply set 40 and perform a saline-only injection.

The user may next install a fluid source container 30 containing a therapeutic or [00252] diagnostic (e.g., pharmaceutical) fluid, such as a contrast bottle. The user typically scans a barcode and like indicia on the fluid source container 30, which is assumed to be contrast media in the present example, using the packaging reader 808 on the mobile support 700. Alternatively the user may use the user interface display 806 to manually indicate that a new contrast fluid source container 30 is being installed and specify the type of contrast, concentration, and container size. If it is not already being displayed on the user interface display 806, the control system 800 next displays a fluid loading screen on the user interface display 806. The control system 800 uses the information from the barcode or like indicia such as an RFID tag in conjunction with an internal database and identifies, for example, the contrast type, iodine concentration, and size of the contrast fluid source container 30 that is to be installed and displays the information on the user interface display 806. The control system 800 indicates on the user interface display 806 that the contrast fluid source container 30 is to be installed in the first or default position "L1" in the left side fluid handling compartment 712 on the mobile support 700. Alternatively, the user may use the user interface display 806 to override this default location and indicate that the contrast fluid source container 30 is being installed in the right side fluid handling compartment 712. This

alternative location may be provided as some users may have a preference to always install the same type of contrast or other fluid on the same side of the mobile support **700**. This override option allows users to install any type of therapeutic or diagnostic (*e.g.*, pharmaceutical) fluid first but still have each type of fluid located in its preferred location. Nonetheless, even with this override option, the first "contrast" fluid source container **30** is installed in the first position "L1" or "R1" in either fluid handling compartment **712** reserved for a therapeutic or diagnostic (*e.g.*, pharmaceutical) fluid, and this position is immediately adjacent the saline support **724** in the fluid handling compartment shown in **FIG. 60**.

The control system 800 again flashes the upper and lower indicator lights 728, 730 that are associated with the selected fluid container support 726 to indicate where the contrast fluid source container 30 should be installed and where the associated fluid supply tube 34 should be used. The user typically removes a protective cap from the top of the contrast fluid source container 30 and cleans the rubber septum. The user may place the contrast fluid source container 30 in the bottle or container support 710 provided on the chosen lateral side of the pedestal 704. The user then makes a fluid connection between the selected "center" fluid supply tube 34 associated with the "center" inlet port 124 on the pump body 100 of the pump 10 and the contrast fluid source container 30 using the spike 36. Depending on the configuration of the fluid supply set 32 provided with the pump 10, as shown in FIGS. 40-43 discussed previously, the user may be required to clean a swabable valve 70 associated with the fluid supply tube 34 and connect a spike 36 thereto to access the contrast fluid source container 30. The user then inverts the contrast fluid source container 30 and inserts the container 30 into the first or "center" fluid container support 726. The "center" fluid supply tube 34 associated with the second or "center" inlet port 124 on the pump body 100 of the pump 10 is now connected to the contrast fluid source container 30 hanging in the center or middle location in the fluid handling compartment 712. In the present example, it may be assumed that the "center" fluid supply tube 34 associated with the second or "center" inlet port 124 on the pump body 100 of the pump 10 is now connected to the contrast fluid source container 30 hanging in the left fluid handling compartment 712. The upper and lower indicator lights 728, 730 associated with the first or center fluid container support 726 remain flashing to guide the user in installing the contrast fluid source container 30 with the correct middle support 726 and, further, guide the user in associating the fluid supply tube 34 with the center or middle air detector 814. The control system 800 detects when the fluid supply tube 34 is installed in the center or middle air detector 814 and enables the "Prime" button on the user interface display 806.

Next, the user presses the "Prime" button on the user interface display 806 to [00254] begin the priming process. The outlet selector valve 280 is rotated to the "waste" position (if not already in position), and the left inlet selector valve 300, based on the foregoing example of locating the contrast fluid source container 30 in the "L1" position in the left side fluid handling compartment 712, is moved from the "OFF" position to a "first" fluid position. In this position, the valve stem 306 of the inlet selector valve body 302 of the left inlet selector valve 300 is rotated by the associated inlet selector valve actuator 464 to permit fluid communication between the second inlet port 324 and the second inlet port 124 on the inlet selector valve cylinder 114 of the pump body 100. Fluid communication is thereby established between the contrast fluid source container 30 and the axial passage 310 in the valve stem 306. One or both of the plungers 200 in the left two (2) pump cylinders 104 of the pump body 100 are retracted to pull air/fluid from the contrast fluid source container 30 into the pump 10 up to a predetermined or preprogrammed priming volume. If the predetermined priming volume may be achieved using one (1) plunger **200**, only one of the two (2) plungers in the left two (2) pump cylinders 104 is actuated. If the predetermined priming volume cannot be achieved with one (1) plunger 200, both left plungers 200 are actuated. The pump cylinder or cylinders 104 on the left side 18 of the pump 10 draw air/fluid from the contrast fluid source container 30, through the fluid supply tube 34 connected to the second inlet port 124 on the inlet selector valve cylinder 114 of the pump body 100, through the left inlet selector valve 300 and left inlet manifold channel 236, and into the left pump cylinder or cylinders 104. At this point, one or both of the two (2) left pump cylinders 104 contain a mixture of air and contrast, and one or both of the two (2) left plungers 200 are advanced, substantially simultaneously, to eject the air/contrast mixture into the waste collection container 48. As this mixture is ejected, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored. If the pressure exceeds a predetermined limit, indicating a blockage in the waste collection tube set 46, the priming process is halted.

[00255] If, in the foregoing process, the final extracted volume (X ml) of air and contrast fluid from the left contrast fluid source container 30 contains less than a predetermined volume of air (Y ml), as determined by the system controller 822 based on sensed air detection information from the associated air detector 814, priming of the fluid supply tube 34 is considered complete. If more than a predetermined volume of air (Y ml) was detected by the system controller 822 based on sensed air detection information from the associated air detector 814, the user is prompted via the user interface display 806 to repeat the foregoing priming process. The control system 800 may also query the user via the user interface

display **806** to visually confirm that the fluid supply tube **34** is free of air and that the priming process is complete. If the user sees air in the fluid supply tube **34**, the user may initiate a repeat of the priming process using the user interface display **806**. In other words, in the contrast priming process, a predetermined volume of air and contrast fluid (X ml) is extracted from the left saline source container **30** and at least a minimum volume (*e.g.*, X ml – Y ml) has to be free of air to consider this priming process complete. The system controller **822** is programmed in advance with information (*e.g.*, X ml and Y ml) that a certain or predetermined volume of fluid must be drawn from the installed contrast fluid source container **30** in order to prime the volume of the fluid supply tube **34**, and can cause the drive pistons **50** to withdraw the plungers **200** a predetermined distance or "stroke" in the pump cylinders **104** to ensure that the predetermined minimum volume of fluid is present for the priming of the fluid supply tube **34**. If for any reason the associated air detector **814** registers the presence of air after the forward or priming stroke of the respective pistons **50**, the system controller **822** will require a repeat of the foregoing priming process.

[00256] Additionally, the control system 800 ideally initiates the clearing of air and contrast from the left inlet selector valve 300 and left inlet manifold channel 236, since it is undesirable to leave contrast in the inlet selector valve 300 or inlet manifold channel 236 as the next injection may use this side of the pump 10 to deliver saline instead of contrast. The left inlet selector valve 300 is moved to the "left saline source" or "S1" position described previously, and the plungers 200 in the two (2) left pump cylinders 104 are retracted substantially simultaneously to pull saline from the left saline fluid source container 30 and into the pump 10 through the fluid path described previously up to a predetermined flushing volume. At this point, both left pump cylinders 104 contain a mixture of air, the contrast that was previously present in the left inlet selector valve 300 and the left inlet manifold channel 236, and now saline. Both plungers 200 are then advanced substantially simultaneously to eject the air/contrast/saline mixture into the waste collection container 48. As this mixture is ejected, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored. If the pressure exceeds a predetermined limit, indicating a blockage in the waste collection tube set 46, the priming process is halted.

[00257] The control system 800 also initiates clearing or purging of air and residual contrast from the outlet manifold channel 244. In this procedure, all four (4) plungers 200 are retracted substantially simultaneously to pull saline from the left saline fluid source container 30 into the pump 10 up to a predetermined flushing volume. All four (4) plungers 200 are then advanced to eject the saline in the pump cylinders 104 into the waste collection

container 48, clearing the outlet manifold channel 244 of air and residual contrast in the process. As this mixture is ejected, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored. If the pressure exceeds a predetermined limit, indicating a blockage in the waste collection tube set 46, the priming process is halted. All four (4) plungers 200 are used for this step, not just the left two (2) plungers 200, because if only the two (2) left plungers 200 are used, residual contrast may be pushed from the two (2) left pump cylinders 104 into the inactive right half of the outlet manifold channel 244. Moving all four (4) plungers 200 forces saline from all four (4) pump cylinders 104 at once, driving any residual contrast or air to the waste collection container 48.

[00258] The fluid supply tube 34 to the left or first contrast fluid source container 30 at position "L1" is primed with contrast and the control system 800 records the installation time of the left contrast fluid source container 30. This recorded information may be displayed for the user on the user interface display 806 or may be viewed automatically or manually at a later point in time, if desired. The control system 800 may also initialize a countdown timer that may be viewed at any time on the user interface display 806 to see the remaining "open life" of the contrast in the left contrast fluid source container 30 based on manufacturer's information or other guidelines for the permitted "open life" of the fluid. The control system 800 may also display expiration warnings on the user interface display 806 when there is less than a predetermined amount of remaining "open life" and when the remaining "open life" has reached zero.

[00259] The control system 800 then moves both inlet selector valves 300 and the outlet selector valve 280 to their "OFF" positions. The control system 800 further changes the upper and lower indicator lights 728, 730 associated with the center or middle fluid container support 726 from flashing to solid, as an example, to indicate that the left contrast fluid source container 30 has been installed, primed, and is ready for use. The user may elect to close the left compartment door 714 to enclose the left fluid handling compartment 712 with the support housing 702. Further, if the convective heating system 734 has been enabled, the control system 800 may engage the heating system 734 to heat the two (2) installed fluid source containers 30. Typically, the heating system 734 heats the air inside of the fluid handling compartment 712 to 40° C and the air inside of the fluid handling compartment 712 is circulated continuously around all of the fluid source containers 30 to warm the fluids. This heating system 734 also heats any fluid source containers 30 that may have been placed in the various supports/hangers 724, 726 even if they are not installed and primed. When the compartment door 712 is in the closed position, the temperature of the air inside of the fluid

handling compartment 712 may be displayed on the user interface display 806 and is continuously monitored by the control system 800. If desired, the fluid delivery system 2 may now be used to perform patient injections using contrast and/or saline, or additional fluid source containers 30 may be installed.

If it is desired to load additional fluid source containers 30, these containers 30 may be installed whenever the fluid delivery system 2 is not performing a fluid injection. For example, additional fluid source containers 30 may be installed prior to performing any fluid injection, or may be installed after some fluid injections have been performed but before the existing fluid source containers 30 are empty. If an additional saline fluid source container 30 is installed in the "right saline source" position or "S2" position in the right fluid handling compartment 712, the foregoing procedure followed to install the "left saline source" or "S1" position is essentially repeated with the right saline fluid source container 30, and both "sides" of the pump 10 are still used during this second saline priming process since the "right saline source" or "S2" must be used to prime both inlet selector valves 300 and the saline channel 132 of the saline manifold 130 for right saline fluid source container 30. If an additional contrast fluid source container 30 is installed, the foregoing process for installing the contrast fluid source container 30 in the first or default position "L1" in the left side fluid handling compartment 712 on the mobile support 700 is followed for installing a second contrast fluid source container 30 in the first or default position "R1" in the right side fluid handling compartment 712 on the mobile support 700.

[00261] In the foregoing example of the fluid delivery system 2 comprising the pump 10, drive and actuating system 400, mobile support 700, and control system 800, there may be several limitations on where contrast fluid source containers 30 may be installed. The first contrast fluid source container 30 is installed in the first or default position "L1" of the left fluid handling compartment 712. If a second contrast fluid source container 30 is to be installed and contains a different type and/or concentration of contrast than the first contrast fluid source container 30, this second contrast fluid source container 30 is installed in the opposite side "R1" position of the right fluid handling compartment 712. In many operation scenarios, all contrast sources in a given fluid handling compartment 712 are of the same type and concentration (but bottle size may vary). Thus, if the second contrast fluid source container 30 is of the same type and concentration as the first, it is typically installed in the second position "L2" of the left fluid handling compartment 712. It is possible, and may be desirable, to install the same type and concentration of contrast in both fluid handling compartments 712 and this has the advantage of providing a greater volume of available

contrast. Accordingly, for each fluid handling compartment 712, it is not permissible, according to the foregoing exemplary implementation of the fluid delivery system 2 comprising saline and contrast fluids, to install contrast in the "L2" or "R2" position unless the same type and concentration of contrast has previously been installed in the "L1" or "R2" positions. As noted previously, if desired, the same type of fluid may be present in all four (4) installed fluid source containers 30 in locations L1, L2 and R1, R2.

[00262] Once both compartment doors 714 are closed to enclose the fluid handling compartments 712 within the support housing 702 and the convective heating system 734 is enabled, the control system 800 may engage the heating system 734 to heat any installed fluid source containers 30. Typically, the heating system 734 heats the air inside of the fluid handling compartment 712 to 40° C and the air inside of the fluid handling compartment 712 is circulated continuously around all of the installed or stored fluid source containers 30 to warm the fluids. When the compartment doors 714 are in the closed position, the temperature of the air inside of the respective fluid handling compartments 712 may be displayed on the user interface display 806, as noted previously.

Typically, the user will specify a patient protocol that is used to perform a fluid [00263] injection. This protocol may be specified before, during, or after the process of installing a pump 10 and the fluid source containers 30. The patient protocol programming may occur concurrently with the installation of the pump 10 or fluid priming processes if the patient protocol is programmed using a remote display screen 904 as shown in FIG. 46B, which may be located in, for example, a control room. The local user interface display 806 is desirably available for installation of the pump 10 and the foregoing fluid priming processes. There may be several different options available for patient protocol entry including, but not limited to: (1) manually programming the patient protocol, specifying the relevant parameters for each phase (fluid type, flow rate, volume, etc.); (2) recalling a previously stored patient protocol from the memory of the control system 800 (or the system controller 822) and the recalled protocol may be used as is or modified by the user before use; and (3) using installed software to have the control system 800 generate a recommended protocol based on the patient's height, weight, type of scan, type of contrast being used, etc. Such system installed software may be adopted from United States Patent No. 5,687,208, incorporated herein by reference, or adopted from one or more of United States Patent Application Publication Nos.: 2007/0282263; 2008/0097197; 2010/0030073; 2010/0113887; and 2010/0204572, also each incorporated herein by reference. If all of the parameters of the entered patient protocol are

acceptable, the control system **800** accepts the patient protocol and allows the user to return to the "Home Screen".

[00264] Next, the user may elect to install and prime a patient supply set 40. The user first cleans the swabable valve 274 located in the patient outlet port 270 on the outlet selector valve cylinder 264 on the manifold plate 230. The user typically scans a barcode and like indicia on the packaging containing the patient supply set 40 using the packaging reader 808 on the mobile support 700. As an alternative, the user may use the user interface display 806 to indicate that a patient supply set 40 is being installed and then manually enter the indicia information. The control system 800 next automatically displays a "Patient Supply Set" installation screen on the user interface display 806. The system controller 822 decodes the indicia information and indentifies the type/configuration, serial number, manufacturing lot number, etc. of the patient supply set 40. The system controller 822 may check the serial number against an internal database. If the serial number is already in the internal database of "used" patient supply sets 40, the system controller 822 generates an error message on the user interface display 806 to indicate that the patient supply set 40 cannot be used. Otherwise, the patient supply set 40 installation process continues.

[00265] The user opens the packaging and removes the patient supply set 40. An indicator LED or other similar lighted device (not shown) may be provided on the patient outlet air detector 810, and may be flashed to remind the user to install the tubing of the patient supply set 40 in the air detector 810. The user attaches the patient supply set 40 to the swabable valve 274. The connector ends 42 of the patient supply set 40 may be color-coded different colors, with one of the colors matching the color of the swabable valve 274 to guide the user in proper connections for the patient supply set 40. If it is not already accomplished, the user installs the tubing of the patient supply set 40 in the air detector 810. The control system 800 desirably detects the presence of the patient supply set 40 in the patient outlet air detector 810 and confirms that the tubing does not contain fluid. If the tubing does contain fluid, the control system 800 may be programmed to assume that the user has accidentally re-installed a used patient supply set 40, issues a warning, and requires removal of the patient supply set 40 before proceeding further.

[00266] Next, the control system 800 displays the priming controls on the user interface display 806 for priming the patient supply set 40. The user holds the free end of the patient supply set 40 over a suitable collection container, and presses the "Prime" button on the user interface display 806. The control system rotates the outlet selector valve from "OFF" to "Patient" to align the flow passage 290 in the valve stem 286 of the outlet selector valve body

282 of the outlet selector valve 280 with the patient outlet port 270 on the outlet selector valve cylinder 264 on the manifold plate 230. The control system 800 also rotates the right inlet selector valve 300 from "OFF" to permit fluid communication between the saline port 332, 334 active for saline supply, namely the right saline source "S2" in the foregoing example. One of the two (2) plungers 200 on the right side 16 of the pump 10 is retracted, drawing saline into the pump cylinder 104, and the plunger 200 is pushed forward to eject the saline through the outlet manifold channel 244 and into the patient supply set 40. As the saline is ejected, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored. If the pressure exceeds a predetermined limit, indicating a blockage, the priming process is halted. As the saline is ejected, the control system 800 monitors the output air detector signal from the patient outlet air detector 810. The final ejected air and liquid volume (e.g., "X ml") is monitored and must contain less than a predetermined volume of air (e.g., "Y ml"). The exact prime volumes (e.g., X ml, Y ml) depend on the specific configuration of patient supply set 40 (e.g., diameter, length, etc.). The user may be prompted to visually confirm that the entire patient supply set 40 has been primed and confirm the priming by pressing a button on the user interface display 806. The user may optionally press a "Small Prime" button on the user interface display 806 to deliver a small amount of additional priming fluid. This option may only appear on the user interface display 806 after the foregoing standard or "full" priming process has been completed. The control system 800 rotates the outlet selector valve 280 from "Patient" back to "OFF", and rotates the right inlet selector valve 300 back to "OFF". The free "patient" end of the patient supply set 40 is secured until the patient is ready for a fluid injection.

[00267] Once the patient supply set 40 is primed, the fluid delivery system 2 may be used in a fluid injection procedure. The user attaches the free or "patient" end of the primed patient supply set 40 to a catheter inserted into the patient. Once all of the patient protocol criteria to perform a patient injection have been met, as described previously, the control system 800 enables an "Arm" button on the "Home Screen", which was previously "grayed-out" and inoperable. Once the "Arm" button is pressed, the control system 800 may perform several final checks, including, but not limited to: (1) confirming that the entered patient protocol is valid; (2) confirming that a sufficient volume of each fluid type has been loaded to execute the patient protocol; in making this determination, the control system 800 may also consider the amount of saline that will be required to flush the pump 10 after the fluid injection; (3) confirming that there is sufficient capacity in the waste collection container 48 to flush the pump 10 after the fluid injection; (4) performing a series of safety checks to ensure that all

sensors and like electronic elements of the fluid delivery system 2 are operating properly; and (5) locking out certain capabilities, such as preventing the addition of additional fluid sources, and preventing the patient protocol from being changed, edited, etc.

[00268] If all of the final checks are successfully performed, the control system 800 indicates that it is in an armed state and enables a "Start" button, which the user presses to execute the programmed patient protocol. The user interface display 806 is updated to indicate that the fluid delivery system 2 is injecting fluid. The outlet selector valve 280 is moved from the "OFF" position to the "Patient" position, and one or both of the inlet selector valves 300 are moved from the "OFF" position to enable fluid communication to the appropriate fluid source container(s) 30. Which inlet selector valves 300 are moved depends upon the specific patient protocol and whether one or two types of fluid are required.

[00269] If it is assumed that two fluids, contrast and saline as in the foregoing example, are to be injected, one plunger 200 on each half of the pump 10 is retracted to fill with fluid. The distance that each plunger 200 is retracted varies with the specific patient protocol. The filling time is minimal and may be on the order of about 2.50 seconds, which includes the time required for the outlet and inlet selector valves 280, 300 to open. One or both of the retracted plungers 200 now moves forward to eject fluid, which is dependent on the specific parameters of the patient protocol. While the initial plungers 200 are ejecting fluid, the "second" or "tandem" plungers 200 in each half of the pump 10 begin to retract and fill their pump cylinders 104 with fluid. This filling process is completed before the moving or ejecting plungers 200 reach the end of their pumping strokes. The two (2) plungers 200 in each half of the pump 10 continue to alternate back and forth in tandem as the fluid injection progresses.

[00270] The overall speed of the plungers 200 in each half of the pump 10 may be independently adjusted upward and downward throughout the fluid injection, as required, to meet the desired flow rate for each patient protocol phase. For many phases, the plungers 200 on one side of the pump 10 may be halted if that side of the pump 10 is not required to deliver fluid during a protocol phase. Throughout the fluid injection procedure, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored by the control system 800. If the outlet pressure in the pressure sensing port 296 begins to near a predefined set point, 300 psi as an example, the velocity of all of the plungers 200 is reduced until the pressure is remains below the defined limit. The velocity of the plungers 200 is dynamically controlled by the control system 800 so that the predefined pressure set point is

not exceeded. If the control system **800** is unable to maintain the sensed pressure below a predetermined safe limit, the fluid injection is aborted.

Additionally, throughout the fluid injection, the patient outlet air detector 810 is monitored, and this information is combined with information about the prevailing flow rate and fluid pressure to calculate the volume of air that has been detected. When one or more air bubbles with a total predetermined volume have been detected, the control system 800 may be programmed to abort the fluid injection. In other words, once a predetermined total "allowable" volume of air has been detected as having passed through the patient outlet air detector 810, the control system 800 is operable to abort the fluid injection. Further, throughout the fluid injection, the control system 800 monitors the "inlet" air detectors 812-816. Any air output signals of inactive fluid source containers 30 (those not currently being used to fill the pump 10) are ignored, while the air output signals from the "inlet" air detectors 812-816 associated with the active fluid source containers 30 are combined with information on the prevailing filling flow rate to calculate the total volume of air that has been detected (if any). When one or more air bubbles with a total predetermined "allowable" volume have been detected in a given fluid supply tube 34, the control system 800 typically performs one of two actions. First, if a second fluid source container 30 of the same fluid type has been installed and primed, the control system 800 can automatically rotate the appropriate inlet selector valve 300 to access this secondary source. Second, if a second fluid source container 30 of the same fluid type is not available, the control system 800 aborts the fluid injection.

[00272] After execution of the programmed patient protocol is completed, the control system 800 moves the inlet selector valves 300 to their "OFF" positions. The control system 800 continues to monitor the pressure in the pressure sensing port 296 and, once the pressure has dropped to nearly zero, the outlet selector valve 280 is moved from "Patient" to "OFF". If the pressure does not dissipate within a predetermined period of time, the outlet selector valve 280 is moved from "Patient" to "Waste" to permit the pressure to dissipate, and then the outlet selector valve 280 is moved to the "OFF" position. The control system 800 indicates to the user via, for example, the user interface display 806 that the fluid injection is complete and summary information on the completed fluid injection may be presented on the user interface display 806. The user may indicate if another fluid injection is desired for the same patient. In this case, the user programs or selects the desired patient protocol and "arms" the fluid delivery system 2 for the next fluid injection. The control system 800 can

track the total volume of each fluid delivered to a patient. If the user specifies a new patient, then these totals are cleared and the pump 10 is flushed.

[00273] The control system 800 next typically automatically performs a flushing process to remove residual contrast from the inlet selector valve 300 and the inlet manifold channel 236 that delivered the contrast in the fluid injection procedure. For this flushing procedure, the outlet selector valve 280 is moved to the "waste" position. The inlet selector valve 300 that was used to deliver contrast during the fluid injection is moved to the saline port 332, 334 for the active saline fluid source container 30. Saline is pulled into one of the pump cylinders 104 on the side 16, 18 of the pump 10 that previously delivered contrast, clearing the inlet selector valve 300 of residual contrast, and drawing the contrast into the pump cylinder 104. The saline and contrast mixture is then ejected from the pump cylinder 104 into the waste collection container 48. There are several possible flush options available including, but not limited to, flushing after each fluid injection, flushing after each patient is completed, and flushing whenever the there is a switch from using one type of fluid such as contrast to another (e.g., when switching from contrast A to contrast B or vice versa).

[00274] The control system 800 next typically automatically performs a flushing process to remove residual contrast from the pump cylinders 104. The plungers 200 are retracted simultaneously for both of the pump cylinders 104 on the side 16, 18 of the pump 10 that previously delivered contrast, pulling saline into the pump cylinders 104. Both plungers 200 are then advanced substantially simultaneously to eject the saline and contrast mixture from the pump cylinders 104 into the waste collection container 48. This flushing process may be repeated as necessary to remove residual contrast from the pump cylinders 104.

[00275] Further, the control system 800 performs a flushing process to remove residual contrast from the outlet manifold channel 244. In this procedure, all four (4) plungers 200 are retracted substantially simultaneously, pulling saline into the pump cylinders 104. Next, all four (4) plungers 200 are advanced substantially simultaneously to eject fluid from the pump cylinders 104 into the waste collection container 48. The user may now disconnect the patient supply set 40 from the patient catheter, disconnect the patient supply set 40 from the swabable valve 274 in the patient outlet port 270, and discard the patient supply set 40 as medical waste.

[00276] Moreover, the user may also want to remove the pump 10 from the drive and actuating system 400. As the final fluid injection ends, all four (4) plungers 200 are fully inserted into their corresponding pump cylinder 104. The control system 800 may indicate to the user that the pump 10 has expired due to the number of patients processed, use time

expiration, or a total maximum number of fluid source containers 30 have been installed, or the user may have simply decided that no further procedures are going to be done. The user indicates on the user interface display 806 that the pump 10 is to be removed. The control system 800 ensures that the pump cylinders 104 are empty of fluid and the inlet selector valves 300 and the outlet selector valves 280 are in their "off" positions. The control system 800 retracts all four (4) piston linear actuators 462, either together or one at a time, to their rear-most positions of the normal working stroke. At this point, the plungers 200 remain attached to the drive pistons 50 associated with the piston linear actuators 462 and are pulled back as well. The control system 800 retracts each piston linear actuator 462, for example, one at a time, and the plungers 200 attached to the drive pistons 50 until the rear or proximal end disc 208 on each plunger 200 contacts a stripper pin (not shown) or like structure that is provided in the drive and actuating system 400. The striper pin prevents the plunger 200 from moving backwards any further. As the piston linear actuator 462 continues to move rearward, the plunger 200 is stripped-off the drive piston 50. The plunger 200 remains in place in the pump cylinder 104 as the piston linear actuator 462 continues to retract. The foregoing process is repeated for the remaining plungers 200.

[00277] In a fluid injection procedure, a fluid source container 30 may often be fully consumed. Thus, it is desirable to replace the spent fluid source container 30 with a new container 30. In certain of the configurations of the pump 10 shown in FIGS. 40-43, it is not advisable or allowable to replace a fluid source container 30. For example, if a fluid spike 36 is permanently attached to the fluid supply tube 34, the spike 36 cannot safely be used more than once. If the spike 36 is removable, the used spike 36 may be removed, along with the used fluid source container 30, and discarded. The swabable valve 70 may then be cleaned and a new spike 36 installed. A new fluid source container 30 of the same fluid type and concentration may then be installed in the same location. Based on the type or configuration of the pump 10, from the pump indicator plate 170 and/or identifying indicia 172, the control system 800 detects which spikes 36 are permanently attached and which are replaceable. The control system 800 may be configured to not permit the user to install a replacement source in a location with a permanently attached spike 36. Additionally, the control system 800 may not permit the user to install a different type of therapeutic or diagnostic (e.g., pharmaceutical) fluid, for example, a different type or concentration of contrast. The replacement fluid source container 30 is to be of the same type and concentration as that which was previously installed in the location.

As mentioned in the foregoing, fluid source containers 30 may be replaced [00278] whenever the fluid delivery system 2 is not performing a fluid injection. Fluid source containers 30 may also be replaced or added whenever the control system 800 is in a programmed hold phase during a fluid injection. A programmed hold phase temporarily suspends the fluid injection process until the user presses the "Start" button to resume the fluid injection. If a saline fluid source container 30 is replaced, the foregoing saline priming sequence is essentially repeated with the new saline fluid source container 30, and both fluid circuits on the two (2) sides 16, 18 of the pump 10 are used during this saline priming process since the new saline fluid source container 30 is used to prime both inlet selector valves 300 and the saline channels 132, 134 and any air that is introduced to the pump 10 is removed. If a replacement contrast fluid source container 30 is installed, the foregoing "contrast" priming sequence is essentially repeated for the appropriate location and appropriate side of the pump 10. While the foregoing discussion was related to saline and contrast fluids as the applicable fluids for use in the pump 10, this specific combination should not be considered limiting. While saline may likely be needed for any fluid injection procedure, the foregoing example using contrast media is intended to be exemplary and any therapeutic or diagnostic (e.g., pharmaceutical) fluid may take the place of contrast media typically used in medical imaging procedures.

[00279] The control system 800 also allows the user to set an adjustable pressure limit. The pressure limit is typically used to ensure that the fluid pressure delivered to the attached catheter remains below the catheter manufacturer's specified maximum pressure rating. The pressure presented to the catheter is largely dependent on the flow rate of the fluid delivered by the fluid delivery system 2. The control system 800 uses the pressure sensor output signal from the pressure measurement mechanism 552 to dynamically reduce the flow rate of the injected fluid as required to ensure the specified pressure limit is not exceeded. The pressure measurement mechanism 552 may also be used to compensate for flow-rate fluctuations that can occur with the multi-stroke plunger - pump cylinder configuration of the pump 10.

[00280] As represented in the accompanying figures, the pump 10 uses two (2) tandem piston operated plungers 200 to deliver a substantially constant flow of fluid from one or more connected fluid source containers 30 to a patient. As shown in FIGS. 61-62, under typical operating conditions, in a tandem plunger 200 – pump cylinder 104 arrangement, as a first plunger 200 begins to decelerate at the end of its pumping or ejection stroke, the second plunger 200 accelerates to reach its target velocity. This is shown in FIG. 61 with the velocity profile of the first plunger 200 – pump cylinder 104 identified by reference character

"P1" and the velocity profile of the staggered or second plunger 200 – pump cylinder 104 identified by reference character "P2". The resulting combined output flow rate from the pump 10 is shown in FIG. 62 and is substantially continuous. The output flow rate is proportional to the sum of the velocities of the two (2) plungers 200 or, more precisely, the sum of the absolute values of the velocities of the two (2) plungers 200. Therefore, as one plunger 200 – pump cylinder 104 ("P1") ejects fluid to the patient, the adjacent plunger 200 pump cylinder 104 ("P2") fills with fluid from the same fluid source container 30. During a brief transition period, the nearly-empty ejecting plunger 200 - pump cylinder 104 decelerates and the newly-filled plunger 200 - pump cylinder 104 accelerates and begins ejecting fluid. By controlling the acceleration and deceleration of the plungers 200, a nearly constant net outlet flow-rate is achieved, as shown in FIG. 62. However, due, in part, to pressure-dependent compliances in the fluid delivery system 2, the accelerating plunger 200 does not deliver fluid immediately and a brief fluctuation in flow rate can occur during the transition period. Since the ejection delay of the accelerating plunger 200 is dependent on the instantaneous outlet pressure of the pump 10 as measured in the pressure sensing port 296 of the outlet selector valve cylinder 264 on the manifold plate 230, the control system 800 can use the pressure sensor output signal from the pressure measurement mechanism 552 to monitor the pump outlet pressure in the pressure sensing port 296, which is in fluid communication via the connecting passage 268 with the outlet manifold channel 244, and dynamically advance the timing of the accelerating plunger 200 as required to minimize the flow-rate fluctuation. The control system 800 may be programmed to predict the amount of fluctuation that will most likely occur, based on prevailing conditions, and take corrective action before the fluctuation occurs.

[00281] The pressure measurement mechanism 552 can also be used to detect incomplete filling of the pump cylinders 104 of the pump 10. If the pump cylinders 104 are not completely filled, the patient may not receive the prescribed volume of fluid in the patient protocol. Some conditions that can cause insufficient filling of the pump cylinders 104 include clogged air vents, occluded spikes, and pinched fluid supply tubes 34. If a pump cylinder 104 is not completely full when its plunger 200 begins ejecting fluid, no fluid will be delivered from the pump cylinder 104 until the "under volume" is displaced by the plunger 200. With no fluid being delivered during this period, the outlet pressure of the pump 10 drops. By monitoring the pump outlet pressure in the pressure sensing port 296 via the pressure measurement mechanism 552, the control system 800 can detect the characteristic pressure drop associated with an under-filled pump cylinder 104 and abort the fluid injection

procedure, or initiate compensating measures. Various techniques for identifying and accounting for an under-volume situation or condition are described in further detail herein.

As each pump 10 is disposable and may be used for multi-patient use over an extended period of time, such as 24 hours, it is desirable to minimize the amount of residual contrast media that remains in the pump 10 after each patient procedure if contrast media is the therapeutic or diagnostic (e.g., pharmaceutical) fluid(s) that is to be utilized in the fluid delivery system 2. Residual contrast that is left in the pump 10 has several disadvantages. If contrast is left in the pump 10 for an extended period of time, it is possible for the contrast to crystallize and form iodine salt crystals inside of the fluid conducting passages. This crystallization can result because contrast is a saturated salt solution and even a small amount of water loss may cause crystallization to begin. Additionally, because the pump 10 may be used with more than one type of contrast, it may be desirable to prevent the two types of contrast from mixing. If a small amount of residual contrast of a first type is left in the fluid conducting passages of the pump 10, it may react with contrast of a second type in an undesirable manner. Further, as the pump 10 may be used with more than one type of contrast, it is desirable to minimize the amount of residual contrast of a first type if the subsequent patient injection will use contrast of a different type, as this will minimize the amount of contrast of the first type that the second or subsequent patient receives.

[00283] To achieve the foregoing minimization of residual contrast, the control system 800 may perform a number of steps to minimize the amount of residual contrast that remains in the pump 10 after a fluid injection. For example, the control system 800 may automatically add a final saline flush phase at the end of each patient protocol. This final saline flush phase helps to clear the outlet manifold channel 244 and outlet selector valve 280 of residual contrast. If the user has already programmed a saline flush at the end of the programmed patient protocol, the control system 800 does not need to add an "automatic" saline flush phase. Additionally, at the end of each patient protocol, the control system 800 may end the fluid injection process with all of the plungers 200 in their forward-most positions within the respective pump cylinders 104 (e.g., with empty pump cylinders 104). This forward-most positioning of the plungers 200 in the pump cylinders 104 minimizes the fluid volume that remains in the pump 10 at the end of a fluid injection.

[00284] After a patient protocol is completed, the control system 800 may also automatically load and execute a pre-defined "Pump Flushing Protocol". This flushing protocol may be designed and optimized to remove as much residual contrast as practical without creating a burdensome volume of waste fluid for the waste collection container 48. In

300 and inlet manifold channel 236 from the fluid circuit on the side 16, 18 of the pump 10 that was recently used to deliver contrast. To achieve the desired flushing, the "contrast" inlet selector valve 300 is moved to achieve fluid connection with the current or active saline fluid source container 30, S1 or S2, and the outlet selector valve 280 is moved to the "Waste" position. Both plungers 200 from the "contrast" fluid circuit on the "contrast" side 16, 18 of the pump 10 are retracted substantially simultaneously to pull saline from the current or active saline fluid source container 30 into the pump 10. Both plungers 200 are then advanced substantially simultaneously to eject the contrast/saline mixture into the waste collection container 48. As this mixture is ejected, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored. If the pressure exceeds a predetermined limit, indicating a blockage in the waste collection tube set 46, the flushing process is halted.

[00285] Next, the control system 800 clears residual contrast from the outlet manifold channel 244. The inlet selector valves 300 are both moved to achieve fluid connection with the current or active saline fluid source container 30, S1 or S2. All four (4) plungers 200 are retracted substantially simultaneously to pull fluid from the current or active saline fluid source container 30 into the pump 10. All four (4) plungers 200 are then advanced to eject the saline in the pump cylinders 104 into the waste collection container 48, clearing the outlet manifold channel 244 of contrast in the process. As this mixture is ejected, the pressure sensor output signal from the pressure measurement mechanism 552 is monitored. If the pressure exceeds a predetermined limit, indicating a blockage in the waste collection tube set **46**, the flushing process is halted. All four (4) plungers **200** are used for this step, not just the two (2) plungers 200 on the "contrast" fluid circuit on the "contrast" side 16, 18 of the pump 10 because, if only the two (2) "contrast" plungers 200 are used, residual contrast may be pushed from the contrast-containing pump cylinders 104 into the inactive half of the outlet manifold channel 244. Moving all four (4) plungers 200 substantially simultaneously forces saline from all four (4) pump cylinders at once, driving any residual contrast to the waste collection container 48 which flushes everything substantially simultaneously. The control system 800 then returns both inlet selector valves 300 and the outlet selector valve 280 to their "OFF" positions.

[00286] In addition to the foregoing control features provided by the control system 800, there are several physical features of the fluid delivery system 2 which assist in minimizing residual contrast and flushing. For example, the pump cylinders 104 permit virtually all of the fluid in the pump cylinders 104 to be ejected. The front or distal end disc 206 on each plunger

200 closely matches the internal shape of the distal end 110 of the pump cylinders 104. Additionally, the inlet and outlet check valves 194, 196 are recessed into the front side 140 of the front end plate 102 on the pump body 100, permitting the plungers 200 to be fully inserted into the respective pump cylinders 104. As noted previously, the pump 10 may draw saline from either side 16, 18 of the pump 10 for flushing operations, and the saline manifold 130 with two (2) saline channels 132, 134 allows both pairs of pump cylinders 104 to access either saline fluid source container 30, regardless of its physical location. Moreover, the saline supply ports 332, 334 are located at the rear of each inlet selector valve 300 to permit the entire valve stem 306 to be flushed of contrast. Further, the drive and actuating system **400** includes a drive motor **600**, such as a stepper motor, for automated control of the outlet selector valve 280, permitting the flushing process to occur without user intervention. Furthermore, the fluid delivery system 2 includes a waste collection container 48 to allow the flushing process to occur without user intervention. Without the waste collection container 48, the patient supply set 40 would have to be manually directed to a suitable waste receptacle for the flushing fluid. The volume of the patient supply set 40 may also be minimized to reduce the amount of saline flush that must be administered to the patient at the end of a fluid injection.

While it is known in syringe-based power injector systems to store patient [00287] protocols in system memory for later use, these stored protocols typically indicate whether a given protocol phase required contrast, saline, or a mixture of contrast and saline. When these "legacy" syringe-based power injector systems stored a patient protocol, they typically did not store any information to indicate what specific type of contrast was used in the stored patient protocol. The user often manually recorded which type of contrast was used for each stored patient protocol. The control system 800 automatically stores different fluid type information with each saved patient protocol. When a stored patient protocol is retrieved from system memory, the type, for example contrast brand and concentration, which was stored with the patient protocol is displayed on the user interface display 806. If, for example, the contrast type that was stored with the patient protocol is currently installed on the fluid delivery system 2, the control system 800 adjusts the patient protocol, if necessary, to correspond to the current configuration of fluid source containers 30, even if the current configuration differs from the configuration as originally presented in the stored patient protocol. For example, if a patient protocol was written which specified the use of "Contrast A", which was, at the time the protocol was written, in the fluid circuit on the left side 16 of the pump 10 and, at a later date, the same patient protocol is recalled but "Contrast A" has

been installed in the fluid circuit on the right side **18** of the pump **10** and designated as "Contrast B", the control system **800** can automatically adjust the patient protocol to replace all of the "Contrast A" references with "Contrast B" references.

[00288] In another instance, if, for example, the fluid type that was stored with the patient protocol is not currently installed on the fluid delivery system 2, the control system 800 can recommend to the user the type of fluid, typically the type of contrast, that should be installed and recommend an installation location, if one is available. The user may be given the option to substitute one of the currently installed fluid types for the fluid type that was originally specified for the patient protocol. Moreover, the control system 800 can be configured to display by default only those stored patient protocols that use the currently loaded fluid types. Further, a "show all" option may be provided to view the remaining patient protocols on the user interface display 806 that use other types of fluids.

[00289] As noted previously, when a fluid source container 30 is installed, the control system 800 typically notes the installation time and can track the remaining "open life" of the installed fluid source container 30 based on the manufacturer's instructions or other guidelines for use, as described previously. Once a fluid source container 30 is installed and primed, the control system 800 can (but is not limited to): (1) record the installation time; (2) use manufacturer's information or other guidelines for the fluid to look up, for example in an internal database, the recommended or permitted open life for the fluid; (3) track the remaining open life for the fluid and display the remaining open life for each fluid source container 30 on the user interface display 806; (4) provide an alert to the user on the user interface display 806 when there is less than a predetermined amount of time remaining in the open life of the fluid; (5) notify the user on the user interface display 806 once the remaining open life has expired and optionally provide the user the option of continuing to use the fluid source container 30 or disabling the fluid source container 30; and (6) automatically switch to another fluid source container 30 if another fluid source container 30 of the same fluid type and concentration has already been installed.

[00290] As also described previously, when a new fluid source container 30 is installed on the fluid delivery system 2, the control system 800 recommends, typically via the user interface display 806, a specific location where the fluid source container 30 should be installed. This recommendation is determined by the location and types of existing fluid source containers 30 that have already been installed, the type of new fluid that is being installed, and prior programming of how the fluid delivery system 2 is typically used. For example, when installing a saline fluid source container 30, if no saline sources have yet been

installed, the control system 800 indicates that the first saline source container 30 is to be installed in the left side fluid handling compartment 712 in the rearmost "S1" location provided by the saline support or hanger 724, as the physical geometry of the pump 10 indicates that saline be installed in this position to support initial priming and flushing procedures. If two (2) saline fluid source containers 30 are currently installed, the control system 800 indicates that there are currently no available open locations to install additional saline. Depending on the configuration of the pump 10 as determined from the associated fluid supply set 32, the user may elect to remove and replace one of the existing saline fluid source containers 30. Alternatively, if one (1) of the two (2) saline fluid source containers 30 is empty, the control system 800 recommends the empty location for installation of the new saline source. The recommended location is indicated by flashing or blinking the upper and lower indicator lights 728, 730 associated with the saline support or hanger 724, and this recommended location may also be graphically indicated on the user interface display 806. When installing contrast, if no contrast fluid source containers 30 are installed, the control system 800 indicates, typically via the user interface display 806, that the contrast fluid source container 30 is to be installed in the first or default "L1" position in the left side fluid handling compartment 712. The upper and lower indicator lights 728, 730 associated with the recommended "L1" position, flash or blink to indicate the recommended installation location. If contrast of the same type and concentration has already been installed, the control system 800 recommends, typically via the user interface display 806, that the new fluid source container 30 be installed in the same fluid handling compartment 712 as the previous container 30 of the same type. Alternatively, if there is an empty fluid source container 30 in the selected fluid handling compartment 712, the control system 800 recommends, typically via the user interface display 806, this location for installation of the new fluid source container 30. If two (2) contrast fluid source containers 30 are currently installed in the selected fluid handling compartment 712, the control system 800 indicates, typically via the user interface display 806, that there are currently no available open locations to install additional fluid source containers 30. Depending on the configuration of the pump 10 as determined from the associated fluid supply set 32, the user may elect to remove and replace one of the existing contrast fluid source containers 30 or install the contrast in the other fluid handling compartment 712. If the new fluid source container 30 contains a different type or concentration than the original fluid source container 30, then several options are available. For example, if contrast fluid source containers 30 have not yet been installed in one of the

fluid handling compartments 712, the control system 800 recommends, typically via the user

interface display **806**, installing the new fluid source container in the "L1" or "R1" positions in the "unused" fluid handling compartment **712**. If contrast fluid source containers **30** have already been installed in both fluid handling compartments **712**, the control system **800** indicates that it is not possible to install the new contrast fluid source container **30**. Thus, if four (4) fluid source containers **30** are already installed, no new containers **30** may be installed, and if one (1) of the four (4) positions is empty and the new contrast type scanned by the user matches the contrast type already installed on that half of the fluid delivery system **2**, the user is permitted to install the new fluid source container **30**.

[00292] Because the fluid delivery system 2 may comprise a pump 10 having several different configurations based on the associated fluid supply set 32, the control system 800 can identify the type of pump 10 that is being used and appropriately limit the fluid delivery system 2 to avoid potential safety issues, particularly for multi-patient use situations. Various configurations or versions of the pump 10 are shown in FIGS. 40-43, which comprise different configurations or versions of the associated fluid supply set 32. There are several types of limits that may be imposed based on the type or configuration of the pump 10 that is installed. In one limitation, the total volume of fluid may be limited based on the type or configuration of the pump 10 and, thus limit the total volume delivered to each patient. This total volume limitation helps ensure that components of the disposable pump 10 are not subjected to excess levels of wear. For example, the distal end lip seal 218 and/or rear or proximal bead seal 220 of the plungers 200 of the pump 10 are subjected to wear and fatigue, respectively, that is roughly proportional to the volume of fluid delivered, and limiting the total volume delivered can help to ensure that excess wear/fatigue levels are not reached that cause failure of the foregoing seals 218, 220. It may be desirable to manufacture the pump 10 with different types of materials, perhaps more robust materials, so that the pump 10 may support a greater number of patient procedures or a greater volume of fluid.

[00293] Additionally, the control system 800 may limit the number of patients that may be connected to a given disposable pump 10. For example, the control system 800 may limit the total number of patients that may be used with each configuration of the pump 10 (see FIGS. 40-43 described previously). This limitation may be set to ensure that components of the disposable pump 10 are not subjected to excess levels of wear. For example, components of the pump 10, such as the outlet selector valve 280, inlet selector valves 300, and the swabable valves 70 are subjected to wear that is roughly proportional to the number of fluid injection procedures that are conducted, and limiting the total number of patients for a given pump 10 can help to ensure that excess wear/fatigue levels are not reached. The risk of external

contamination also increases with the number of fluid connections that are made. Again, it may be desirable to manufacture the pump 10 with different types of materials, perhaps more robust materials, so that the pump 10 may support a greater number of patient procedures or a greater volume of fluid.

[00294] The control system 800 may also limit the total number of fluid connections made with the pump 10. As discussed previously in connection with the configurations of the pump 10 shown in FIGS. 40-43, some of the associated fluid supply sets 32 have permanently attached spikes 36 that can only be safely used with a single fluid container. Once a fluid source container 30 is installed on a permanently attached spike 36, no additional fluid source containers 30 may be installed on that spike 36. Because the permanent spikes 36 are only designed for one use, re-using a spike 36 with a second fluid source container 30 could possibly introduce contamination into the fluid path. When a pump 10 is installed, the control system 800 identifies the configuration of the pump 10 via the pump indicator plate 170 and/or the identifying indicia 172. If the installed pump 10 has permanently attached spikes 36, the control system 800 may be programmed to permit the user to install one fluid source container 30 at each location with a permanently attached spike 36, and if the user tries to install a second fluid source container 30 on a permanently attached spike 36, the control system 800 may be programmed to not permit the second container 30 to be primed and used. As a comparison, configurations of the pump 10 that have swabable valves 70 may have the associated spikes 36 removed and replaced with new spikes 36. Replaceable spikes 36 allow fluid source containers 30 to be removed and safely replaced with new fluid source containers **30** and replacement spikes **36** for sterility purposes. The control system **800** can also impose a practical limit on the number of replacement fluid source containers 30 that may be installed when a spike 36 is replaced with each new fluid source container 30 to limit the potential wear and potential contamination of the swabable valves 70.

[00295] Further, the control system 800 may limit the total "open life" of the pump 10. The "open life" or permitted use limit of the pump 10 may be pre-limited by the programming of the control system 800 to ensure sterility during use. While the configurations of the pump 10 (see FIGS. 40-43) are expected to have a certain minimum "open life", for example 24 hours, it is also possible and desirable to develop additional configurations that would have a longer open life. For example, it may be possible to modify the materials used in the pump 10, such as by including silver ions, to help the internal fluid passages of the pump 10 to remain sufficiently sterile over a longer period of time.

Moreover, the control system 800 may limit use of the pump 10 based on the [00296] patient supply set 40 that is installed on the pump 10. To prevent cross-contamination between patients, it is desirable for the control system 800 to require that the patient supply set 40 be replaced after each patient. For example, the control system 800 can monitor the status of the patient outlet air detector 810 to determine if the patient supply set 40 has been replaced after each patient. If the patient supply set 40 is properly replaced, the control system 800 can infer, based on the status of the patient outlet air detector 810, that a new and unused patient supply set 40 has been installed. The patient outlet air detector 810, as well as the inlet air detectors 812-816 each typically include a tubing latch to hold the tubing of the patient supply set 40 or the fluid supply tubes 34. Electronic signals regarding the status of this latch (e.g., closed or open) and whether fluid is detected in the tubing loaded therein can be used by the control system **800** to determine whether the status of the patient supply set **40** or the fluid supply tubes 34. In the case of the patient supply set 40, it is desirable to know that a new and unused patient supply set 40 has been installed and primed. For example, the control system 800 may be programmed to confirm that a sequence of events has occurred that indicates that the patient supply set 40 has been replaced. For example, this sequence may include, but is not limited to: (1) determining that the latch is closed and fluid is detected in the tubing; (2) determining when an injection has ended and prompting the user to replace the patient supply set 40; (3) determining that the latch is open and air is detected in the tubing; (4) determining that the latch is closed and air is detected in the tubing; (5) determining that the sequence for priming the patient supply set 40 has been accomplished; and (6) determining that the latch is closed and fluid is present in the tubing. Failure to detect the foregoing states or steps from the patient outlet air detector 810 may indicate that the patient supply set 40 has not been replaced. For example, if a tubing latch on the patient outlet air detector 810 is opened and closed, but the new tubing is filled with fluid prior to priming, it may be inferred that the user has removed and re-installed the used patient supply set 40 in the patient outlet air detector 810. Alternatively, a "tubing present sensor" may be used in place of a latch which allows the control system 800 to determine whether the air detector 810 has tubing installed. The inlet air detectors 812, 814, 816 may have latches or could utilize either molded detents or spring clips to hold tubing in place. In the present embodiment, the 812, 814, 816 have small spring-loaded pins (not shown) that allow the control system 800 to determine if tubing has been installed in a particular inlet air detector 812, 814, 816.

[00297] In a variation of the use limitation for the patient supply set 40, the total "open life" of the patient supply set 40 may be used to limit use of the pump 10. As with the pump 10, each patient supply set 40 has a manufacturer's recommended predetermined safe "open life". Beyond this "open life", it may no longer be possible to assure sufficient sterility for patient use. The control system 800 can determine when a particular patient supply set 40 has been installed and track its remaining safe "open life". Again, it may be desirable to provide the patient supply set 40 made from materials suitable for extending "open life", such as using silver ion impregnated polymeric material. Additionally, it may be possible to limit use of the pump 10 based on performance limits of the patient supply set 40. While one specific and non-limiting embodiment of the patient supply set 40 is shown in FIG. 44, discussed previously, several different types or embodiments of the patient supply set 40 may be provided based on desired performance characteristics, which may be encoded in a bar code or like indicia on the packing of the patient supply set 40 and/or on the patient supply set 40 itself. Upon identifying the type or configuration of the patient supply set 40, the control system 800 can adjust performance limits accordingly. For example, the patient supply set 40 may be provided in varying lengths. As such, because the tubing volume varies with length, the control system 800 may adjust the required priming volume and initial fluid delivery delay adjustment based on the tubing length. Alternatively, the patient supply set 40 may have varying constructions, and various types of the patient supply set 40 may have different pressure ratings and the like. If some of the configurations or types of the patient supply set 40 are stronger and less compliant than others, the control system 800 can permit these "reinforced" patient supply sets 40 to operate at higher delivery pressures. Further, a patient supply set 40 with a smaller diameter bore could be provided for low flow rate procedures to provide improved flexibility, reduce the amount of flush that must be delivered to the patient at the end of each fluid injection to clear the patient supply set 40, and provide a faster response time at the beginning of each fluid injection, since the smaller tube volume means less time is required for the fluid to reach a patient.

[00298] In known syringe-based power injector systems, the user is often able to set a pressure limit for the system. During the patient procedure, the system controller monitors the pressure in the syringe and limits the delivered flow rate to ensure that the pressure in the syringe does not exceed the programmed pressure limit. A limitation of this approach is that the pressure limit generally must be set according to the pressure rating of the patient's catheter. For example, if the catheter has a maximum pressure rating of 300 psi, the user configures the system to limit the pressure in the syringe to 300 psi. While this strategy

prevents the catheter from being over pressurized, it also limits system performance since the actual pressure at the catheter is typically much lower than the catheter's pressure rating. The cause of this discrepancy is due to the frictional losses that occur in the tubing that connects the syringe to the catheter. At high flow rates with high viscosity fluids, the pressure drop in the tubing may be more than 100 psi. Because the system measures and regulates pressure at the syringe, this has the effect of reducing the available pressure at the catheter.

The present fluid delivery system 2 provides an improved approach. In operation, the control system 800 measures the pressure in the pressure sensing port 296 in the outlet selector valve cylinder 264 on the manifold plate 230 which supports the outlet selector valve body 282 of the outlet selector valve 280. Using knowledge of the instantaneous flow rate and properties of the fluid that is being delivered, such as viscosity and density, the control system 800 can estimate the pressure drop that will occur in the patient supply set 40. The estimate may either be performed with analytically derived equations based on fluid mechanics or by extrapolating from empirically derived laboratory data. The control system **800** estimates the pressure at the catheter hub by subtracting the estimated pressure drop from measured pressure. The estimated pressure at the catheter is used as an input to the control system 800. If the current flow rate is at the targeted/programmed flow rate and the estimated catheter pressure is at or below a predefined pressure limit, the flow rate is the targeted/programmed flow rate. If the estimated catheter pressure is greater than the predefined pressure limit, the actual flow rate is decreased from the targeted flow rate using a control algorithm, such as a Proportional-Integral-Derivative ("PID") control algorithm which is programmed into the control system 800, such as into the system controller 822. If the estimated catheter pressure is less than the predefined limit and the current flow rate is below the target flow rate, the current flow rate is increased using a control algorithm, such as the PID control algorithm. The control algorithm dynamically adjusts to changes in the flow rate and the transition of fluid types and resulting change in viscosity and density within the patient supply set 40. By correcting for frictional losses in the patient supply set 40, the foregoing approach maximizes the flow rate delivered by the fluid delivery system 2.

[00300] As described in the foregoing, the disposable pump 10 typically has a total "open life" in which the safety and sterility of the pump 10 can be reasonably assured. Accordingly, since the safety and sterility of the pump 10 can only be assured for a limited period of time after installation, the pump 10 may incorporate features to ensure that the pump 10 is not used beyond its safe life as recommended by the manufacturer or by other guidelines. For example, the control system 800 may be programmed to not permit a used pump 10 to be

reinstalled after its total "open life" has expired. The control system **800** can track and record the pump serial number of each pump **10** that is installed in the drive and actuating system **400** and prevent the user from reinstalling the same pump **10** at a later date. One method for preventing such inappropriate and potentially harmful reuse is to position the inlet selector valves **300** to guard against the possibility that a used pump **10** may be installed at a later time in the same fluid delivery system **2** or another such system **2**.

For example, when a pump 10 is assembled and manufactured, desirably in an automated assembly and manufacturing process, a random valve position number between 1 and N (inclusive) may be selected, with "N" representing the N possible combinations of the angular positions of the valve stem 306 of the inlet selector valves 300. Each inlet selector valve 300 may be assembled in any one of \sqrt{N} possible angular positions, yielding $\sqrt{N} \times \sqrt{N} =$ N possible positions for the combination of the left and right inlet selector valves 300. The automated manufacturing process combines the randomly selected valve position number, the sequential pump serial number, the manufacturing batch/lot number and other data, such as the product expiration date, manufactured date, etc., and generates an encoded or encrypted data string. This data string is printed on the pump body 100, desirably as both a humanreadable string and as a machine-readable barcode or like machine-readable indicia, as the identifying indicia 172 and/or as part of the pump indicator plate 170. A manufacturing station in the process reads the identifying indicia 172 and/or the pump indicator plate 170 on each assembled pump 10, extracts the valve position code, and inserts the left and right valve stems 306 of the inlet selector valves 300 into the respective left and right inlet selector valve cylinders 114 on the pump body 100 in the specified angular orientations. The pump 10 may then be packaged, sterilized, and shipped to an end user.

[00302] When a user installs a pump 10 in the drive and actuating system 400, the user opens the package and scans the identifying indicia 172 on the pump body 100 using the packaging reader 808 on the mobile support 700. Alternatively, the user may manually enter the character string located on the identifying indicia 172 on the pump body 100 using the user interface display 806. The system controller 822 receives the information contained in the identifying indicia 172 and extracts the pump serial number and valve position code, and other relevant information as described previously. If the pump serial number corresponds to the serial number of a pump that was previously used in this particular fluid delivery system 2, the control system 800, typically the system controller 822, rejects the pump 10 and generates a message to the user. If the pump 10 has not been previously used in this fluid delivery system 2, the system controller 822 rotates the left and right inlet selector valve

actuators 464 to correspond to the angular positions of the valve stem 306 of the inlet selector valve body 302 of the inlet selector valves 300 indicated by the valve position code. The user may then insert the pump 10 into the drive and actuating system 400 since the orientation of the inlet selector valves 300 will now match that of inlet selector valve actuators 464 and the pump 10 will fit into the pump cradle 412 in the drive and actuating system 400 and the pump drawer 402 may be properly closed and locked.

[00303] When a user wants to remove a "used" pump 10 from the pump drawer 402, the user indicates, via the user interface display 806, that he/she wishes to remove the pump 10. The control system 800 actuates the left and right inlet selector valve actuators 464 to position the valve stem 306 of the inlet selector valves 300 to their "OFF" positions. This "OFF" position may be provided so that it does not correspond to any of the possible initial angular orientations of the valve stems 306 of the inlet selector valves 300 for a "new" pump 10. The user then removes and properly discards the "used" pump 10.

When a user attempts to re-install a "used" pump in a different fluid delivery system 2, the user scans the identifying indicia 172 on the pump body 100 of the "used" pump 10 using the packaging reader 808 on the mobile support 700. The system controller 822 receives the information contained in the identifying indicia 172 and extracts the pump serial number and valve position code, and other information as described previously. Since the pump serial number does not correspond to a pump serial number of a pump 10 that was previously used in this specific fluid delivery system 2, the system controller 822 "accepts" the pump 10. The system controller 822 rotates the left and right inlet selector valve actuators 464 to correspond to the angular positions of the valve stem 306 of the inlet selector valve body 302 of the inlet selector valves 300 indicated by the valve position code for a "new" pump 10, as indicated by the valve position code derived from the identifying indicia 172. If the user attempts to load the pump 10 into the drive and actuating system 400, the drive and actuating system 400 will not physically "accept" the pump 10 because the valve stems 306 of the respective inlet selector valves 300 are set to their "OFF" positions, and this positioning does not match that of the left and right inlet selector valve actuators 464, which have been set to positions corresponding to the encoded angular positions indicated by the "read" valve position code, and the pump drawer 402 cannot be fully closed by the user.

[00305] In the foregoing, while a bar code was generally described as one possible implementation for the identifying indicia 172 on the pump body 100, this may be replaced by a writeable RFID tag on the pump body 100 in the same location, if desired. If a rewriteable RFID is used, the RFID tag can track the uses by decrementing or incrementing a

count after each use until a maximum number has been reached or the counter reaches zero. As alternatives, the counter may be decremented/incremented after each patient procedure until a maximum number has been reached or the counter reaches zero. When the counter reaches a maximum or zero, the pump 10 cannot be used again as this "prior-use" information is locally stored on the pump 10. As noted in the foregoing, once the pump 10 is installed into a fluid delivery system 2, the control system 800 initiates a timer to limit the total amount of time the pump 10 may be exposed to the operational environment. When this timer expires, the control system 800 can prevent further patient procedures from being initiated with that pump 10. A display of the pump time remaining and uses may be displayed to the user on the user interface display 806.

[00306] In known syringe-based power injector systems, conventional optical and ultrasonic air detection devices are typically used to detect the presence of air in medical tubing sets. These sensors are generally only able to detect the presence or absence of air within their detection field and they are not able to measure the quantity of air that has been detected. As a result, when a conventional air detector indicates the presence of air, the injector system typically halts the injection process, regardless of the volume of air involved. In the present fluid delivery system 2, while conventional optical or ultrasonic air detectors may be used for air detectors 810-816, these air detectors 810-816, in conjunction with other elements of the fluid delivery system 2, can be used to measure and track the amount of air that has been observed passing through the patient supply set 40 and the fluid supply tubes 34 of the various fluid supply sets 32 that may be associated with the pump 10. By measuring the quantity of air that has passed through the various medical tubes in the fluid delivery system 2, the control system 800 can operate the fluid delivery system 2 to provide enhanced performance.

[00307] For example, during most venous computed tomography (CT) injections, a very small amount of injected air can be tolerated without adverse effects. In many situations, the harm of aborting a fluid injection due to the detection of a small amount of air may be more detrimental than the potential harm of actually injecting a small amount of air into a patient. In these instances, it is often preferable to continue with the fluid injection instead of aborting the fluid injection if the volume of air may be measured and is determined to be small. This behavior helps reduce the number of "nuisance alarms". It also enables the control system 800 to confirm priming by assuring that the fluid volume necessary to prime the tubing downstream from the air detector(s) 810-816 has passed free of an unacceptable amount of air.

[00308] During a fluid injection procedure, the system controller 822 of the control system 800 may monitor several different "air detection channels" and track the cumulative volume of air that has been detected in each channel. Several input parameters or signals may be used by the system controller 822 in the calculation process, including, but not limited to: (1) the six (6) total air detector signals from the respective inlet air detectors **812-816** in the two (2) lateral fluid handling compartments 712 indicating the presence of air in the respective fluid supply tubes 34 connected to the pump 10; (2) the two (2) angular position signals from angular position sensors 494 associated with the two (2) inlet selector valves 300 and which are connected to the sensor control board 804; (3) the motor direction of the four (4) piston drive motors 442 that provide the motive forces for operating the respective piston linear actuators 462; and (4) a motor encoder count as determined by a drive motor encoder 826 associated with each of the four (4) piston drive motors 442 that records an encoder count each time the piston drive motor 442 advances or retracts, for example, advances or retracts a distance equivalent to 0.075 µL of displacement of the plungers 200 in the respective pump cylinders **104** of the pump body **100** of the pump **10**.

[00309] In the foregoing, if a particular inlet selector valve 300 is in the "OFF" position, it may be assumed that this valve 300 cannot be contributing to an increase in the cumulative volume of measured air. Additionally, in the foregoing, the direction of one or more of the piston drive motors 442 may be assessed and, for example, if a particular piston drive motor 442 is moving forward, then the signal from the associated drive motor encoder 826 is not considered in the calculation process for measuring air that is being drawn into the pump 10, since this particular piston drive motor 442 is operating the associated piston linear actuator 462 to move the plunger 200 to eject fluid from the pump cylinder 104 and, hence, is moving in the "wrong" direction.

[00310] In the calculation process for monitoring the several different "air detection channels", the foregoing electronic signal inputs to the system controller 822 of the control system 800 are used. In the calculation process for each of the "air detection channels", if an inlet air detector 812-816 indicates the presence of air in one of the fluid supply tubes 34 connected to the pump 10, and if the left inlet selector valve 300 is in the required angular position, and if the right inlet selector valve 300 is in the required position, and if one of the monitored piston drive motors 442 is moving in the "correct" direction, a cumulative volume of air counted in the system controller 822 for that specifically monitored "air detection channel" is incremented by a predetermined volume, such as $0.075 \mu L$, for each encoder pulse that is detected with the corresponding piston drive motor 442. Once the cumulative

volume of air for a given "air detection channel" has reached or exceeded a predetermined threshold, the control system 800 can command the inlet selector valve 300 to connect the pump 10 to a secondary fluid source container 30 containing fluid of the same type and concentration, if one exists and is available, or abort the fluid injection if no secondary source is available. If no backup fluid source container 30 exists, then the fluid injection cannot be completed since there is insufficient fluid volume available. The foregoing cumulative air detection procedure may be used to confirm that the fluid supply tubes 34 are properly primed when a new fluid source container 30 is installed. During the initial portion of the fluid priming process, the control system 800 can reset the predetermined threshold after the initial air present in the fluid supply tube(s) 34 has been cleared. If the predetermined threshold is exceeded during the remaining bolus of the fluid priming process, the control system 800 can require the priming operation to be repeated. Another approach to the foregoing is to count encoder pulses without air and stop when they exceed the required prime bolus.

[00311] In summary, in the foregoing, the control system 800 typically selects one of the inlet selector valves 300 for examination. The control system 800 then only needs to monitor the inlet air detector 812-816 associated with the active fluid source container 30 (e.g., S1/S2, L1/R1 or L2/R2) associated with the selected inlet selector valve 300. Next, when air is detected, the encoder counts of the two (2) drive motors 442 associated with the selected inlet selector valve 300 (e.g., signal inputs from the two (2) drive motor encoders 826 connected with the two (2) drive motors 442) are added to the "running" air total if the drive motors 442 are moving in the "correct" withdrawing or retracting direction. Once the total of encoder pulses exceeds a predetermined limit (e.g., equivalent to a predetermined air volume), the system controller 822 sends a command to switch to a backup fluid source container 30. If no such source is available, the fluid injection is terminated.

[00312] The process for monitoring the patient outlet air detector 810, which tracks the volume of air that is being delivered via the patient supply set 40, is generally similar to the foregoing process used for the inlet air detectors 812-816, with certain differences. These differences include: (1) the fact that there is only one air detector 810 of interest, so only one "air detection channel" is monitored; (2) only encoder counts/pulses from those piston drive motors 442 causing the connected plunger 200 to eject fluid from the associated pump cylinder 104 are of interest and assessed by the system controller 822, with electronic signals from any other piston drive motor 442 being ignored; and (3) because of the significant pressures in the patient supply set 40, which can be 400-500 psi and greater, the calculation

for the cumulative volume of air should be adjusted for the prevailing fluid pressure. In this latter instance, if, for example, the fluid pressure is 147 psig, the actual air bubble size will be about 1/10th of the air bubble size at atmospheric pressure. Once the permitted predetermined threshold for permitted cumulative air volume has been reached, the fluid injection is aborted by the system controller **822**.

[00313] In known syringe-based power injector systems, the syringe is filled by the user in advance of a patient procedure. During the filling operation, the user confirms that the syringe has been properly filled to the correct volume and does not contain air. Because the present fluid delivery system 2 has, in a desirable embodiment, two (2) tandem plunger 200 – pump cylinder 104 arrangements that deliver fluid continuously, the pump chambers 106 of the pump cylinders 104 are automatically filled immediately before each delivery stroke of the plunger 200. The continuous fluid delivery system 2 comprises certain safeguards to ensure that the proper type of fluid and volume is delivered for each delivery stroke of the plungers 200 in the respective pump cylinders 104. These certain safeguards may include, but are not limited to, monitoring of the piston drive motors 442 that provide the motive forces to the respective piston linear actuators 462 that operate the plungers 200 to confirm that each of the piston linear actuators 462 have moved the appropriate distance to deliver the requested volume.

As noted previously, it is desirable, in the present continuous fluid delivery system [00314] 2, to detect any "under volume" conditions. In an under volume condition, a restriction in the fluid supply path, for example, in the spikes 36, fluid supply tubes 34, pump inlet selector valves 300, inlet check valves 194, etc. can prevent one or more of the pump cylinders 104 from filling completely. The drive and actuating system 400 can still draw the plungers 200 back through the appropriate stroke, but the restriction can prevent the pump cylinder or cylinders 104 from filling completely with fluid in the allotted "fill" time. Instead, in this situation, the pump cylinder 104 typically contains a mixture of fluid and vapor (under vacuum) at the end of the filling operation. When the associated plunger 200 is advanced to eject fluid from the pump cylinder 104, the vapor bubble collapses as the volume in the pump cylinder 104 is reduced and, eventually, any liquid present in the pump cylinder 104 is ejected. However, the requested volume of liquid is not delivered in the ejection or forward stroke of the plunger 200 in the pump cylinder 104. This under volume condition may not be detected by the patient outlet air detector 810 as the pump cylinder 104 does not contain air and no air will be present for detection by the air detector 810. Any vapor bubbles in the pump cylinder 104 collapse and revert back to liquid form before being ejected from the

pump cylinder **104**. To guard against this "under volume" condition, various techniques for identifying and accounting for an under-volume situation or condition may be incorporated into the control system **800**. Typically, the control system **800**, typically the system controller **822**, includes an "under volume detection algorithm" to detect under volume conditions and alert the user. The algorithm may be programmed so that, if the under volume condition is severe enough, the control system **800** may abort the fluid injection.

The under volume detection algorithm may be based one or more methods that may be used to detect an under volume condition during the course of a fluid injection. Referring to FIGS. 63-64, one such detection scheme can be to include an integral force transducer 828 as part of the drive piston 50, as shown in FIG. 63. For example, this force transducer 828 could be a strain gauge that has been incorporated into the distal portion of the drive piston 50 that interfaces with the plunger 200. The force transducer 828 is capable of measuring the linear force that is applied to the corresponding plunger 200 during operation. In "normal" or "typical" operation, the plunger 200 is retracted by the associated piston linear actuator 462 to fill the corresponding pump cylinder 104 as described previously. Once the pump cylinder 104 is filled with fluid, the drive piston 50 is advanced to eject the fluid. As the ejecting or pumping stroke begins, the control system 800 monitors the output of the force transducer 828. If the pump cylinder 104 is properly filled with fluid, the force will immediately begin to ramp upward as shown by curve "C1" in FIG. 64, which is a force vs. displacement graph. Any compliance in the drive and actuating system 400 and/or the pump 10 may cause the force to gradually rise upward (as shown) until the pressure in the pump cylinder 104 matches the pressure in the outlet manifold channel 244. The force of the piston linear actuator 462 typically remains constant for the remainder of the ejection stroke.

[00316] If a restriction exists, as described in the foregoing, the pump cylinder 104 likely contains a mixture of liquid and vapor at the end of the filling cycle. As the plunger 200 is advanced to eject fluid from the pump cylinder 104, the force transducer 828 indicates that little or no force is being applied to the plunger 200 as shown by curve "C2" in FIG. 63. This lack of force is because the plunger 200 is initially compressing the vapor bubble, which requires little or no applied force. Once the vapor bubble is fully compressed and the pump cylinder 104 contains only liquid, the force applied to the plunger 200 begins to rise, as shown by curve C2. Again, any compliance in the drive and actuating system 400 and/or the pump 10 may cause the force to gradually rise upward (as shown) until the pressure in the pump cylinder 104 matches the pressure in the outlet manifold channel 244. The degree of under volume generally corresponds to that portion of the pump cylinder 104 that has not

been properly filled with fluid, and may be estimated by measuring the distance that the plunger **200** moves before the force of the piston linear actuator **462** begins to rise. For example, if the plunger **200** moves approximately 25% of the total ejection stroke before the force begins to rise, it may be inferred that only about three-fourths (3/4) of the requested volume was actually loaded in the pump chamber **106**.

[00317] The under volume detection algorithm may also include a motor current detection scheme in place of or as an augmentation to the foregoing force transducer 828 arrangement to detect an under volume condition during the course of a fluid injection. In this detection scheme, the force transducer 828 is not required for each piston linear actuator 462. Instead, the control system 800, namely the system controller 822, monitors the current drawn by each of the piston drive motors 442 for the respective piston linear actuators 462 as each plunger 200 is advanced within its pump cylinder 104. The current drawn by each piston drive motor 442 is proportional to both the torque that the piston drive motor 442 develops and the linear force that is applied to the associated plunger 200. The under volume detection algorithm may use this motor current information to determine an under volume condition. An advantage of the foregoing motor current detection scheme is that the multiple force transducers 828 which are integrated into the drive pistons 50, as described in the foregoing, can be eliminated, if desired.

[00318] Further, the under volume detection algorithm may also include a pressure waveform analysis detection scheme in place of or as an augmentation to the foregoing motor current detection scheme and/or the foregoing force transducer 828 arrangement to detect an under volume condition during the course of a fluid injection. The pressure waveform analysis detection scheme may be used to detect an under volume condition by continuously analyzing the pressure in the pressure sensing port 296 and, therefore, the outlet manifold channel 244 using the pressure sensor output signal from the pressure measurement mechanism 552, and the system controller 822 looks for trends or changes in the output pressure.

[00319] Referring again to FIGS. 61-62 and further to FIGS. 65-67, the pressure waveform analysis detection scheme may be explained with an example. In this example, it is assumed that only two (2) plungers 200 are being used to deliver fluid. As shown in FIGS. 61-62, described previously, under typical operating conditions, in a two (2) plunger 200 – pump cylinder 104 arrangement, as a first plunger 200 begins to decelerate at the end of its pumping or ejection stroke, the second plunger 200 accelerates to reach its target velocity. This operational state is shown in FIGS. 61-62, with the velocity profile of the first plunger

200 – pump cylinder 104 identified by reference character "P1", and the velocity profile of the staggered or second plunger 200 – pump cylinder 104 identified by reference character "P2". The resulting combined output flow rate from the pump 10 is shown in FIG. 62 and is substantially continuous. The output flow rate is proportional to the sum of the velocities of the two plungers 200 or, more precisely, the sum of the absolute values of the velocities of the two plungers 200.

[00320] Next, a pump 10 with an under volume condition is considered with reference to FIGS. 65-67. In this situation, it may be assumed that the "first" plunger 200 - pump cylinder 104 ("P1") has completely filled as expected but the "second" plunger 200 - pump cylinder 104 ("P2") has not filled completely because of a restriction. In the present example, the degree of under volume is relatively small and only a few milliliters, perhaps 10%-20% of the volume of the pump cylinder 104. Because of the under volume condition, the output flow rate of the second plunger 200 - pump cylinder 104 ("P2") is not proportional to plunger velocity. In FIG. 65, the velocity profile of the second plunger 200 – pump cylinder 104 ("P2") will be as desired, but the output flow rate from the pump cylinder 104 lags behind the plunger velocity as shown with the dashed line in FIG. 65. This lag is present because no fluid is ejected from the pump cylinder 104 until the vapor bubble has been fully compressed and the pressure in the pump cylinder 104 exceeds the pressure in the outlet manifold channel 244. FIG. 66 shows the combined output flow rate for the two plunger 200 - pump cylinder 104 arrangements from FIG. 65, and there is a pronounced "dip" or "sag" in the flow rate profile. The corresponding pressure profile in the outlet manifold channel 244, as measured by the pressure measurement mechanism 552 via the pressure sensing port 296, is very similar in shape to the flow rate profile shown in FIG. 66. FIG. 67 shows the combined output flow rate for a pump 10 in which the second plunger 200 - pump cylinder 104 ("P2") has experienced a severe under volume condition. In this case, the second plunger 200 - pump cylinder 104 ("P2") has been filled to, perhaps, only 60%-70% of full capacity, and the corresponding flow rate and pressure profile "dips" or "sags" are very significant and pronounced.

[00321] The foregoing pressure waveform analysis detection method has the advantages that no additional sensors or transducers are needed in the drive and actuating system 400 beyond those present for normal operation, as described in the foregoing. The calculations to be carried out by the under volume detection algorithm programmed into the system controller 822 are well within the skill of one skilled in the computer arts, and do not have to be performed at an extremely high update rate. A possible disadvantage of the pressure

waveform analysis method is that it may be challenging to detect certain types of under volume conditions, such as at extremely low flow rates when sufficient pressure is not present in the outlet manifold channel 244, or when a fluid mixture operation, for example a mixture of saline and contrast, is being conducted and there may not be a large enough pressure deviation for reliable under volume detection. For example, if saline constitutes 10% of the current phase, it may not be possible to detect an under volume condition in one or more of the "saline" pump cylinders 104 because the "contrast" pump cylinders 104 may be generating the vast majority of the output flow rate and pressure. Further, under volume detection may not be possible for ejection phases that start near a point in the programmed patient protocol where the flow rate is required to change. For example, if the programmed flow rate drops, the control system 800 can expect a sudden decrease in outlet pressure since the overall flow rate of the pump 10 is being intentionally decreased. It may be difficult to distinguish an unexpected drop in outlet pressure due to an under volume condition from an expected drop in pressure due to an intentional programmed change in the flow rate.

[00322] While several assembly steps for assembly the pump 10 have been described in the foregoing, this disclosure now provides further information on the assembly of the pump 10 for us in the fluid delivery system 2. The following discussion is intended as exemplary and non-limiting as to an assembly for process for constructing the disposable pump 10.

[00323] Before beginning assembly of a "batch" or "run" of pumps 10, the operator enters a manufacturing batch number and pump type number into a manufacturing process control computer in a production facility. If the pump sequential identification numbering does not begin with 00001, the starting number is also be specified. The manufacturing process control computer assigns a unique, sequential identification to each pump 10. This number typically begins with 00001 for the first pump 10 of the batch and is incremented by 1 for each subsequent pump 10. Next, the saline manifold cap 136 is installed over the saline manifold channels 132, 134 and is welded, typically laser welded, to the pump body 100. The inlet and outlet check valves 194, 196 are placed in their respective recesses, described previously. The front manifold plate 230 may then be installed onto the pump body 100, capturing the check valves 194, 196 between these two components. The front manifold plate 230 is then welded, typically laser welded, to the pump body 100. An inlet manifold cap 262 is installed onto each of the two channel members 238 forming the respective inlet manifold channels 236.

[00324] The manufacturing process control computer next selects an inlet selector valve position number for each pump 10 and this number may be assigned sequentially starting with 01 for the first pump 10 in the batch and incrementing by one (1) for each subsequent

pump 10. Once a maximum permitted value has been reached, for example 36, the counter is reset back to a value of 01 for the next or 37th pump 10. Alternatively, the manufacturing process control computer may randomly select a number between 01 and a maximum permitted value, for example 36, for the initial angular position of the valve stem 306 of the inlet selector valves 300, instead of sequentially assigning values. The designated inlet selector valve position number is combined with the uniquely-assigned serial number along with other information as desired, such as the manufacturing lot code and pump type/configuration identifier. This combined data is then encoded into a 14-character string. The 14-character data string is used, for example, to create the identifying indicia 172, such as a barcode label, that can be laser-etched directly onto the pump 10, as described previously in this disclosure. The encoded data string is used to generate a corresponding machinereadable barcode matrix, as an example, and the label desirably also contains the same information in human-readable alphanumeric characters. A mist of silicone lubricant may be sprayed onto the interior wall surface of the pump cylinders 104, onto the interior surface of the inlet selector valve cylinders 114, and onto the interior surface of the outlet selector valve cylinder 264 on the manifold plate 230. Next, at a valve insertion assembly station of the manufacturing facility, the manufacturing process equipment reads the identifying indicia 172, such as a barcode label, on the pump body 100, the encoded information is decoded using a decoding algorithm, and the inlet selector valve position number is extracted. The extracted inlet selector valve position number is used in conjunction with a look-up table to determine the assembled positions of the left and right inlet selector valves **300**. For example, if the extracted inlet selector valve position number was 19/36, the valve stem 306 of the left inlet selector valve 300 may be placed in one predetermined position, such as angular position "4" which corresponds to a specific angular orientation of the valve stem 306 in the left inlet selector valve cylinder 114, and the valve stem 306 of the right inlet selector valve 300 may be placed in another predetermined position, such as angular position "1" which corresponds to a specific angular orientation of the valve stem 306 in the right inlet selector valve cylinder 114. Next, the two (2) valve stems 306 and four (4) plungers 200 are loaded into an automated insertion fixture, which uses servomotors to adjust the angular orientation of the left and right valve stems 306 to match the angular positions indicated by the extracted inlet selector valve position number. The automated insertion fixture concurrently inserts both valve stems 306 and all four (4) plungers 200 into the respective inlet selector valve cylinders 114 and pump cylinders 104 on the pump body 100. It will be appreciated that the valve stems 306 and the plungers 200 may be inserted into the respective inlet selector valve

cylinders 114 and pump cylinders 104 on the pump body 100 in a two or more step process, for example, one at a time.

[00325] Additionally, for the outlet selector valve 280, the valve stem 286 of the outlet selector valve body 282 is inserted into the outlet selector valve cylinder 264 on the manifold plate 230. Prior to insertion, the angular orientation of the valve stem 286 is adjusted to ensure that the flow passage 290 is aligned or in fluid communication with the waste outlet port 272 on the outlet selector valve cylinder 264. Next, the fluid supply tubes 34 are attached to the inlet ports 122, 124, 126 on the inlet selector valve cylinders 114 via, for example, integral barbs on the inlet ports 122, 124, 126. Next, the pump indicator plate 170 is installed into the recessed groove 176 on the outside of one of the pump cylinders 104. The indicator plate 170, as described previously, contains grooves 174 which indicate at least the specific pump configuration of the pump 10 based on the associated fluid supply set 32 for the pump 10. The groove pattern 174 in the pump indicator plate 170 matches the configuration of the pump 10 and its associated fluid supply tubes 34 (see FIGS. 40-43). The waste collection tube set 46 with attached waste collection container 48 is attached to the waste outlet port 272 on the outlet selector valve cylinder 264 on the manifold plate 230.

[00326] While embodiments of a fluid delivery system including a fluid pumping device, optionally provided as a disposable pump cassette, and methods of assembling and use and operation thereof were provided in the foregoing description, those skilled in the art may make modifications and alterations to these embodiments without departing from the scope and spirit of the invention. Accordingly, the foregoing description is intended to be illustrative rather than restrictive. The invention described hereinabove is defined by the appended claims and all changes to the invention that fall within the meaning and the range of equivalency of the claims are to be embraced within their scope.

THE INVENTION CLAIMED IS:

1. A fluid delivery system, comprising:

a fluid pump device, comprising:

a plurality of pump cylinders;

a plunger reciprocally operable within each of the pump cylinders; and

an inlet selector valve to establish selective fluid communication

between at least one fluid source container and the pump cylinders, the inlet selector valve

located laterally outboard of the pump cylinders; and

a drive and actuating system to independently and reciprocally operate the plungers in the pump cylinders.

- 2. The fluid delivery system as claimed in Claim 1, wherein the inlet selector valve is oriented generally parallel to the pump cylinders.
- 3. The fluid delivery system as claimed in Claim 1, further comprising a pump manifold controlling fluid communication to the pump cylinders, and wherein the inlet selector valve controls fluid communication with the at least one fluid source to control fluid flow into the pump manifold.
- 4. The fluid delivery system as claimed in Claim 3, wherein the pump manifold comprises an inlet manifold channel and an outlet manifold channel, and wherein the pump cylinders each comprise at least one inlet opening for fluid communication with the inlet manifold channel and at least one outlet opening for fluid communication with the outlet manifold channel.
- 5. The fluid delivery system as claimed in Claim 4, wherein the pump cylinders are in selective fluid communication with the inlet manifold channel and the outlet manifold channel via respective inlet check valves and outlet check valves.
- 6. The fluid delivery system as claimed in Claim 5, wherein the at least one outlet opening is positioned at a high point in each of the pump cylinders for air bubble egress.

7. The fluid delivery system as claimed in Claim 1, wherein the inlet selector valve comprises an inlet selector valve cylinder having a valve stem disposed therein, the valve stem defining an axial passage and a plurality of radial inlet ports connected to the axial passage.

- 8. The fluid delivery system as claimed in Claim 7, wherein the radial inlet ports are disposed at different angular orientations around the valve stem.
- 9. The fluid delivery system as claimed in Claim 7, wherein the valve stem comprises a plurality of radial inlet ports disposed at different angular orientations around the valve stem and at different axial locations along the valve stem.
- 10. The fluid delivery system as claimed in Claim 1, further comprising a saline manifold in selective fluid communication with the pump cylinders via the inlet selector valve to establish selective fluid communication between a saline fluid source and the pump cylinders.
- 11. The fluid delivery system as claimed in Claim 10, wherein the saline manifold extends across the plurality of pump cylinders.
- 12. The fluid delivery system as claimed in Claim 1, wherein the inlet selector valve is operable by the drive and actuating system independently of the plungers.
- 13. The fluid delivery system as claimed in Claim 1, further comprising identifying indicia on the fluid pump device and encoded with identifying information for the fluid pump device.
- 14. The fluid delivery system as claimed in Claim 13, wherein the inlet selector valve comprises an inlet selector valve cylinder having a valve stem disposed therein, the identifying information comprising at least an initial angular orientation of the valve stem in the inlet selector valve cylinder or a representation thereof.
- 15. The fluid delivery system as claimed in Claim 14, wherein the valve stem comprises a plurality of radial inlet ports.

16. The fluid delivery system as claimed in Claim 15, wherein the radial inlet ports are disposed at different angular orientations around the valve stem.

- 17. The fluid delivery system as claimed in Claim 15, wherein the radial inlet ports are disposed at different angular orientations around the valve stem and at different axial locations along the valve stem.
- 18. The fluid delivery system as claimed in Claim 14, wherein the inlet selector valve cylinder is oriented generally parallel to the pump cylinders.
- 19. The fluid delivery system as claimed in Claim 13, wherein the identifying indicia is an optically encoded transparent member.
- 20. The fluid delivery system as claimed in Claim 13, wherein the identifying indicia is disposed on one of the pump cylinders.
- 21. The fluid delivery system as claimed in Claim 1, wherein each of the plungers comprises a piston interface member extending proximally therefrom, and wherein the piston interface member is split into at least two parts that are compressible towards one another.
- 22. The fluid delivery system as claimed in Claim 21, wherein the plungers each comprise a distal end disc and a proximal end disc.
- 23. The fluid delivery system as claimed in Claim 22, wherein the plungers are reciprocally operable in the respective pump cylinders such that the distal end disc of each of the plungers is operable within a pumping zone of the pump cylinders and the proximal end disc is operable within an isolation zone of the pump cylinders.
- 24. The fluid delivery system as claimed in Claim 22, further comprising a seal provided at least circumferentially about each of the distal end disc and the proximal end disc.

25. The fluid delivery system as claimed in Claim 21, further comprising a radial lip on each of the at least two parts to interface with a drive piston of the drive and actuating system.

- 26. The fluid delivery system as claimed in Claim 21, further comprising a support member coaxially disposed in the piston interface member.
- 27. A drive and actuating system for operating a fluid pump device, comprising:

an extendable and retractable pump drawer to accept the fluid pump device, the fluid pump device comprising a plurality of pump cylinders and a plunger reciprocally operable within each of the pump cylinders;

drive pistons adapted for mechanical connection to the plungers, respectively, to independently and reciprocally operate the plungers in the pump cylinders;

piston linear actuators respectively coupled to the drive pistons; and drive motors operatively coupled to the piston linear actuators, respectively, to provide motive forces to the piston linear actuators to independently and reciprocally operate the plungers.

- 28. The drive and actuating system as claimed in Claim 27, wherein the fluid pump device further comprises an inlet selector valve to establish selective fluid communication between at least one fluid source container and the pump cylinders, and wherein the inlet selector valve is located laterally outboard of the pump cylinders.
- 29. The drive and actuating system as claimed in Claim 28, further comprising an inlet selector valve actuator adapted for mechanical connection to the inlet selector valve to control operation of the inlet selector valve to establish the selective fluid communication between the at least one fluid source container and the pump cylinders.
- 30. The drive and actuating system as claimed in Claim 27, further comprising a pump manifold controlling fluid communication to the pump cylinders, and a pump clamping mechanism operable to secure the fluid pump device in the pump drawer and apply a compressive force to the pump manifold when the fluid pump device is loaded in the pump drawer.

31. The drive and actuating system as claimed in Claim 30, wherein the pump clamping mechanism comprises a clamping block to engage the pump manifold when the fluid pump device is loaded in the pump drawer.

- 32. The drive and actuating system as claimed in Claim 31, wherein the clamping block is operated by a clamp actuating mechanism to engage and disengage the clamping block with the pump manifold.
- 33. The drive and actuating system as claimed in Claim 32, wherein the pump manifold comprises a pressure sensing port with a pressure sensing diaphragm, and wherein the drive and actuating system further comprises a pressure measuring mechanism adapted to interface with the pressure sensing port.
- 34. The drive and actuating system as claimed in Claim 33, wherein operation of the clamp actuating mechanism to engage the clamping block with the pump manifold concurrently causes the pressure measuring mechanism to operatively interface with the pressure sensing diaphragm.
- 35. The drive and actuating system as claimed in Claim 27, further comprising a pump manifold controlling fluid communication to the pump cylinders, and wherein the pump manifold comprises a pressure sensing port comprising a pressure sensing diaphragm, and wherein the drive and actuating system further comprises a pressure measuring mechanism adapted to interface with the pressure sensing port.
- 36. The drive and actuating system as claimed in Claim 27, further comprising a pump manifold controlling fluid communication to the pump cylinders, the pump manifold comprising an inlet manifold channel and an outlet manifold channel, and further comprising an outlet selector valve in fluid communication with the outlet manifold channel to control fluid flow from the pump manifold.
- 37. The drive and actuating system as claimed in Claim 36, wherein the drive and actuating system further comprises an outlet selector valve actuator to control operation of the outlet selector valve.

38. The drive and actuating system as claimed in Claim 27, wherein the plungers each comprise a piston interface member split into at least two parts that are compressible towards one another to enable the mechanical connection with the respective drive pistons.

- 39. The drive and actuating system as claimed in Claim 38, further comprising a radial lip on each of the at least two parts to interface with the respective drive pistons.
- 40. The drive and actuating system as claimed in Claim 38, further comprising a support member coaxially disposed in the piston interface member.
- 41. The drive and actuating system as claimed in Claim 38, further comprising a radial lip on each of the at least two parts of the respective piston interface members to interface with a receiving groove in a socket in the corresponding drive pistons of the drive and actuating system.
- 42. A method of interfacing a fluid pump device with a drive and actuating system of a fluid delivery system, comprising:

providing the fluid pump device, comprising:

a plurality of pump cylinders; and

a plunger reciprocally operable within each of the pump cylinders, each of the plungers comprising a piston interface member extending proximally therefrom, and wherein the piston interface member is split into at least two parts that are compressible towards one another; and

interfacing the plungers with respective drive pistons of the drive and actuating system, such that the at least two parts of each of the piston interface members compress towards one another to enable mechanical engagement with the respective drive pistons.

43. A method as claimed in Claim 42, wherein the drive pistons independently and reciprocally operate the plungers in the respective pump cylinders.

44. The method as claimed in Claim 42, wherein the fluid pump device further comprises an inlet selector valve to establish selective fluid communication between at least one fluid source container and the pump cylinders, the inlet selector valve located laterally outboard of the pump cylinders.

- 45. A method as claimed in Claim 42, wherein the plungers each comprise a distal end disc and a proximal end disc.
- 46. The method claimed in Claim 45, wherein the plungers are reciprocally operable in the respective pump cylinders such that the distal end disc of each of the plungers is operable within a pumping zone of the pump cylinders and the proximal end disc is operable within an isolation zone of the pump cylinders.
- 47. The method as claimed in Claim 45, further comprising a seal provided at least circumferentially about each of the distal end disc and the proximal end disc.
- 48. The method as claimed in Claim 42, further comprising a radial lip on each of the at least two parts of the respective piston interface members to interface with a receiving groove in a socket in the respective drive pistons of the drive and actuating system.
- 49. The method as claimed in Claim 42, further comprising a support member coaxially disposed in the piston interface member.
- 50. The method as claimed in Claim 42, further comprising a radial lip on each of the at least two parts of the piston interface members, and the respective drive pistons each comprising a distal end socket defining a receiving groove, such that the step of interfacing the plungers with the respective drive pistons comprises receiving the piston interface members into the distal end socket in the respective drive pistons and engaging the radial lip on the at least two parts with the receiving groove in the distal end socket in each of the respective drive pistons.

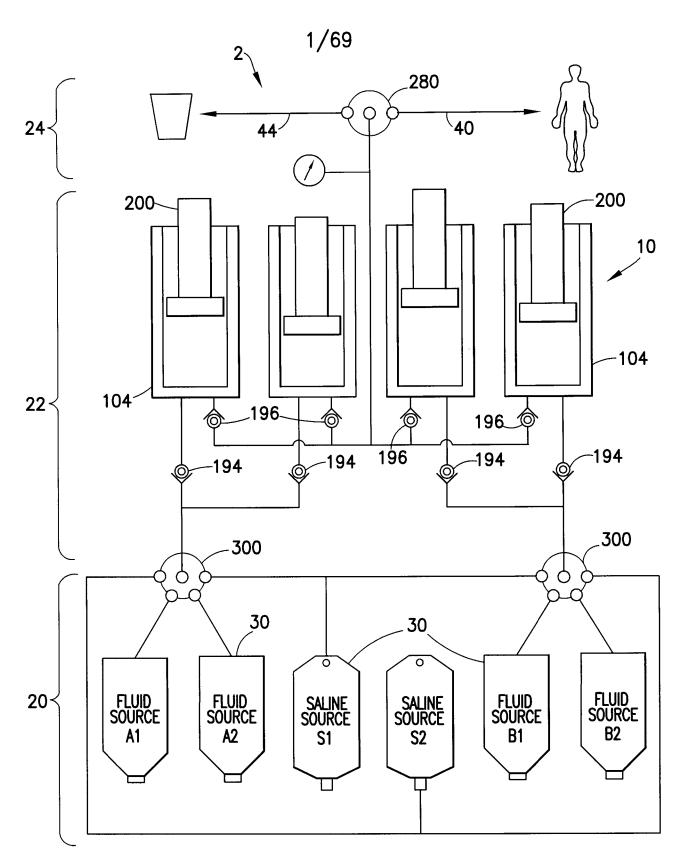
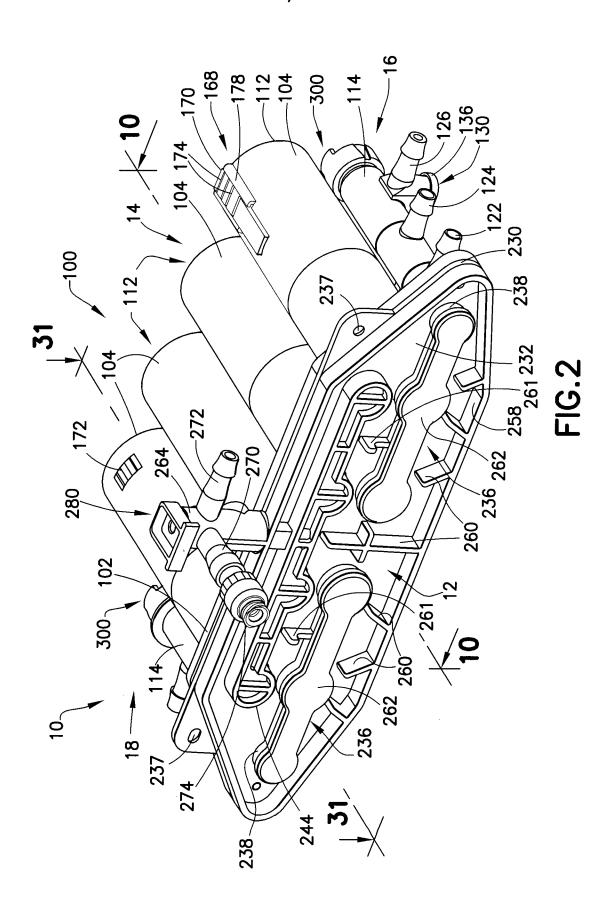
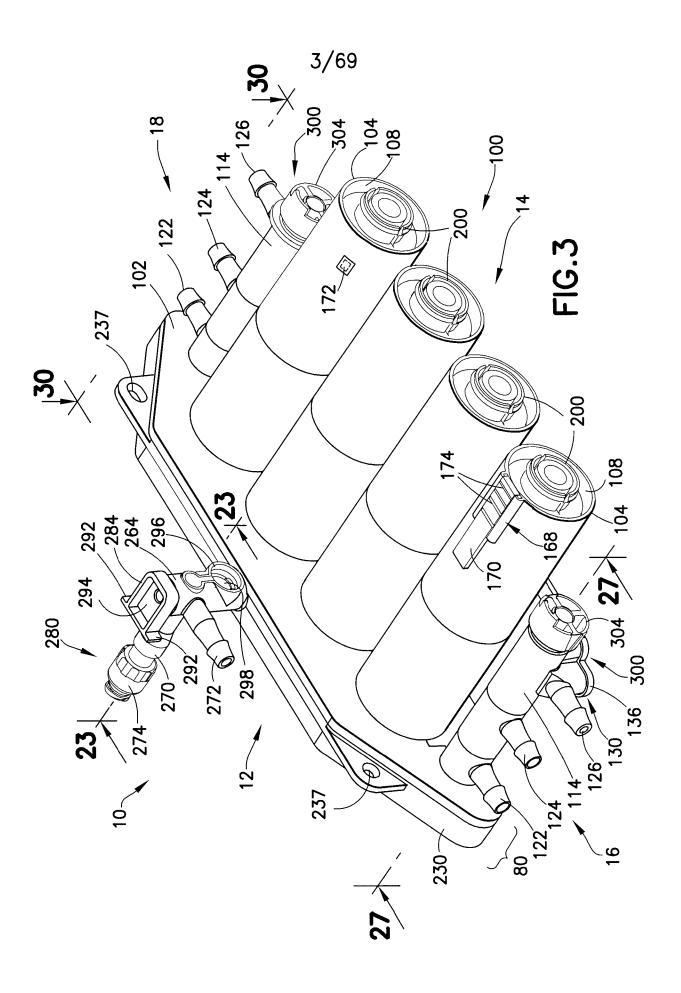
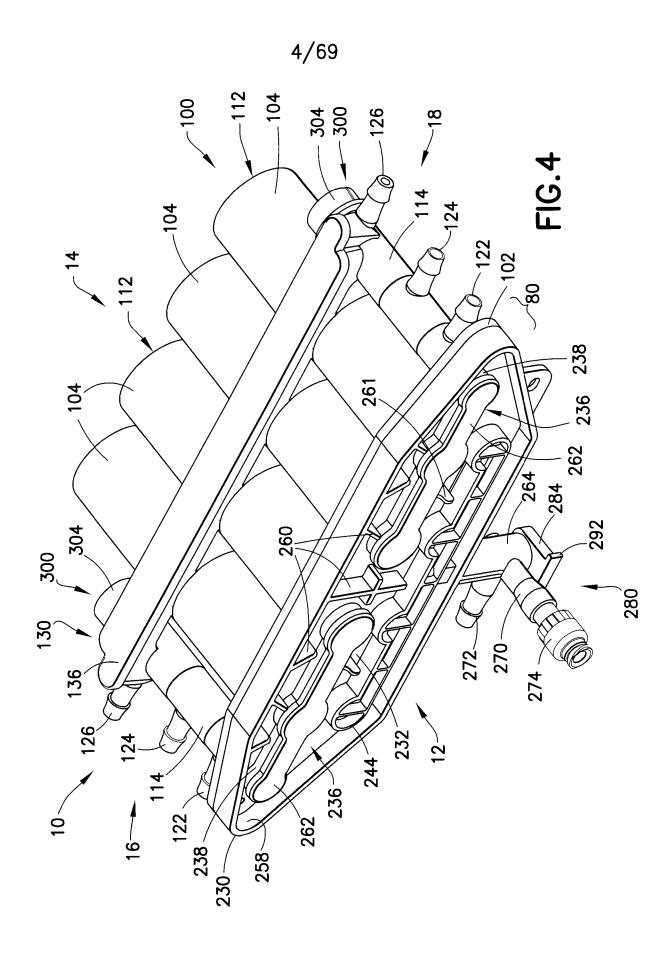


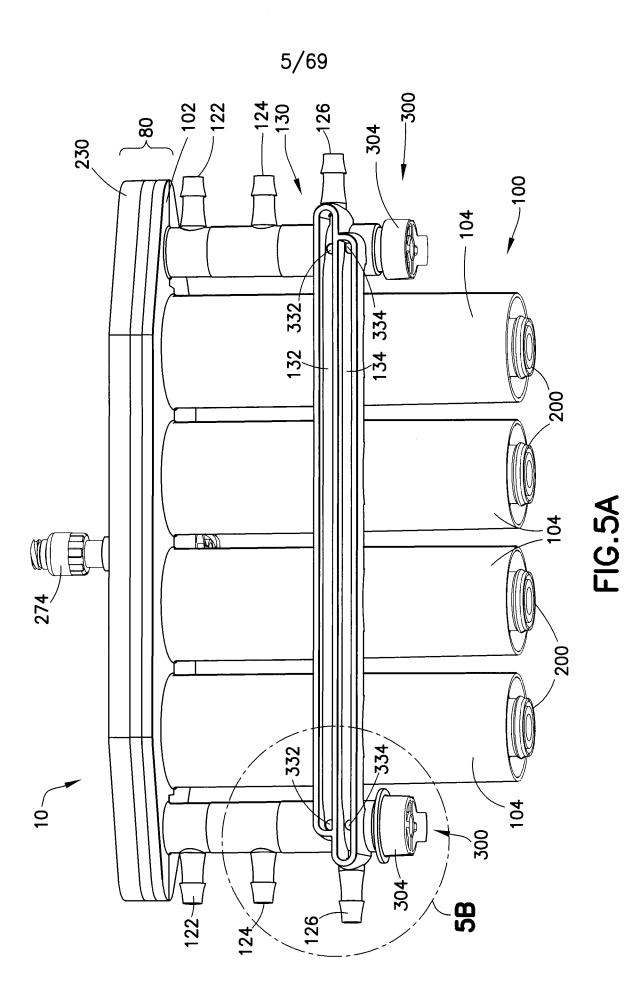
FIG.1

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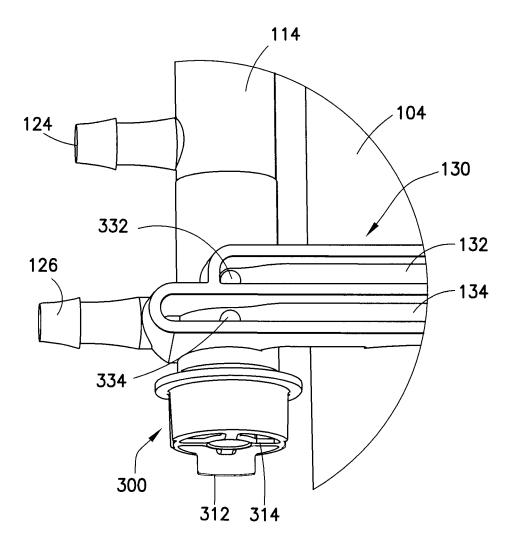
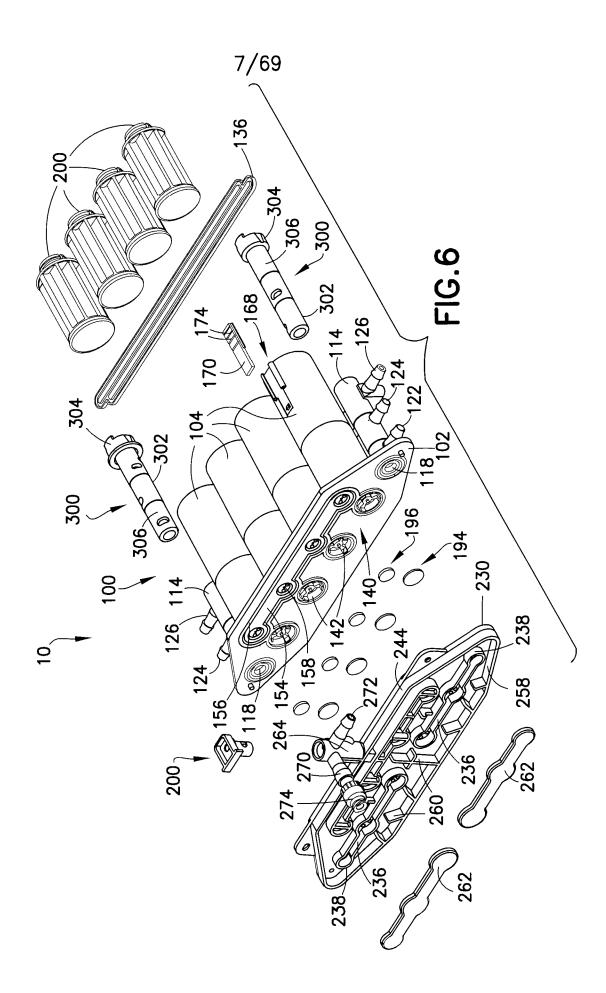
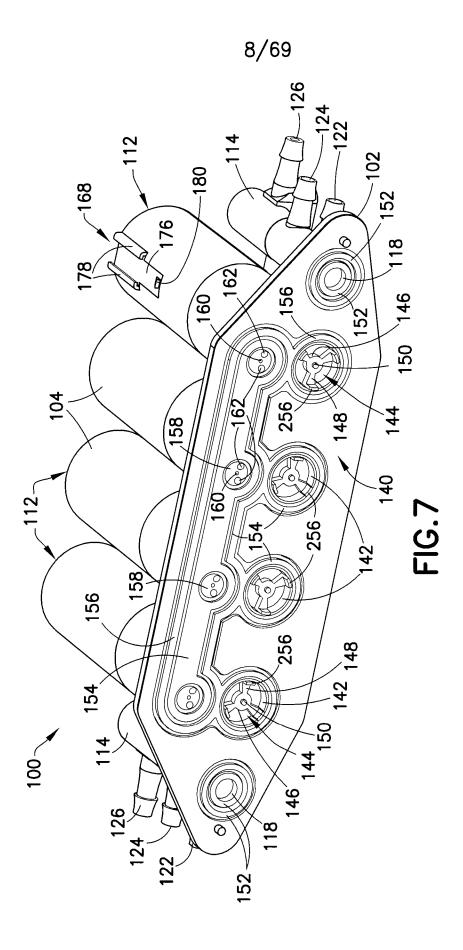
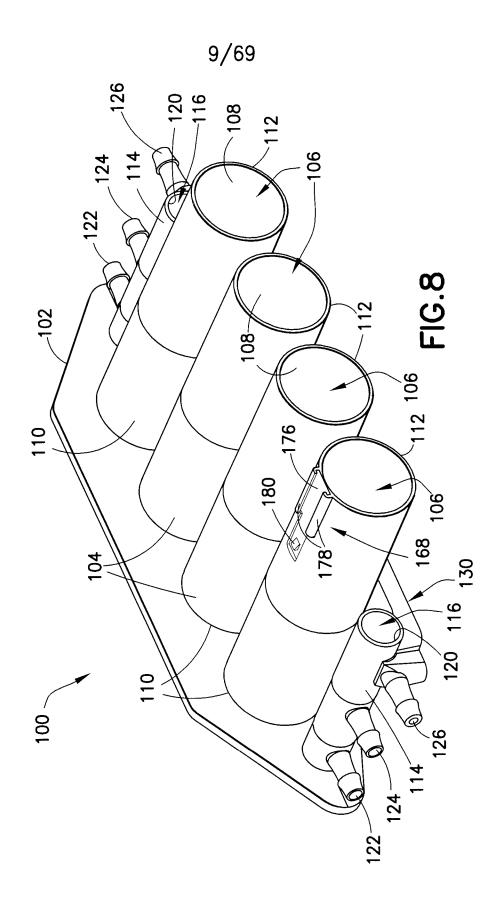
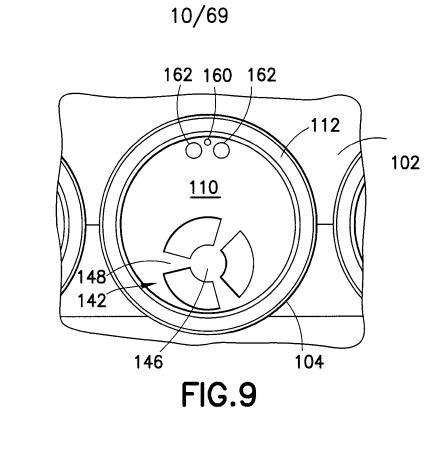


FIG.5B

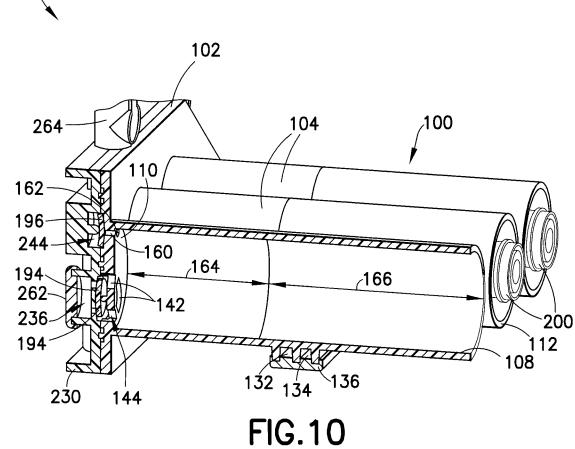


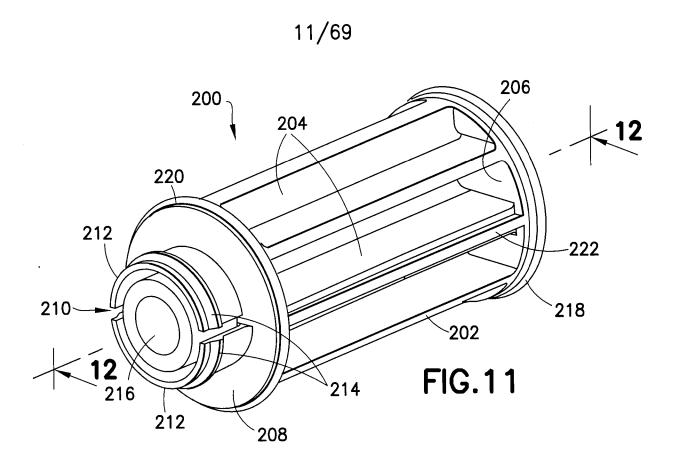


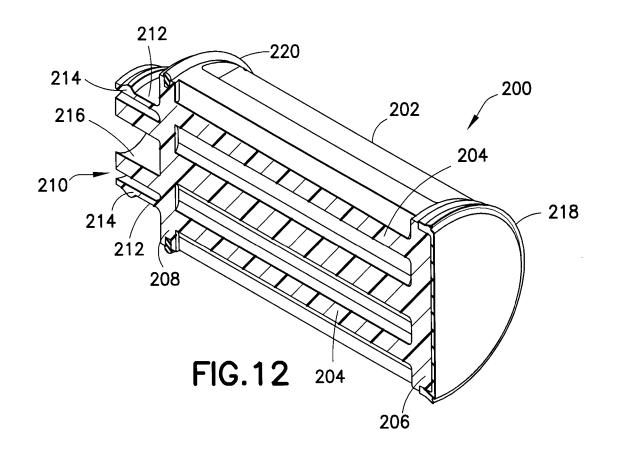




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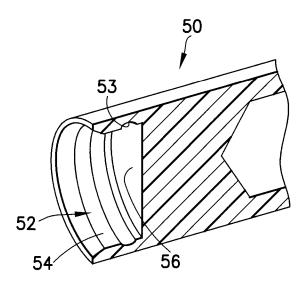
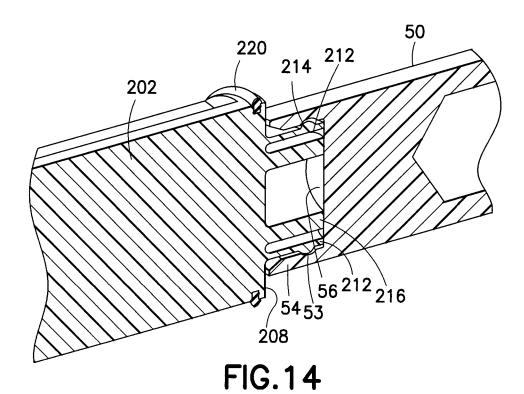
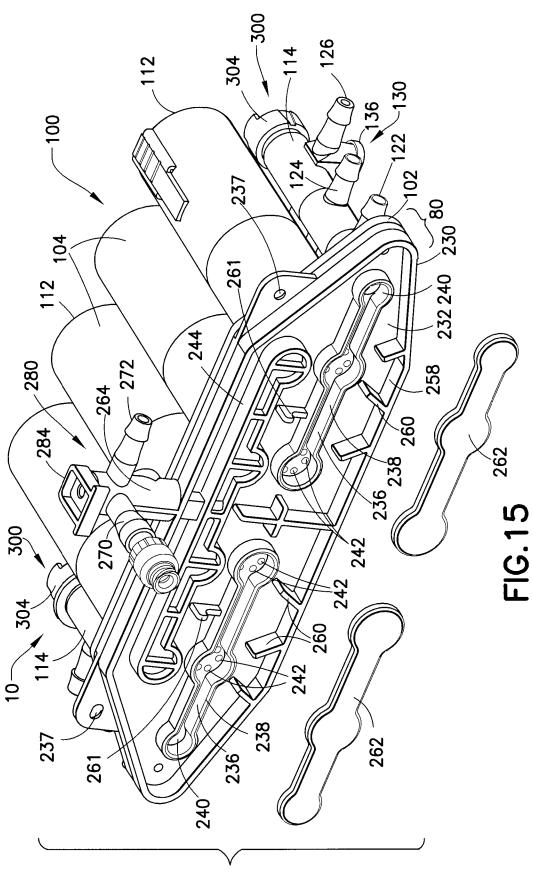


FIG.13







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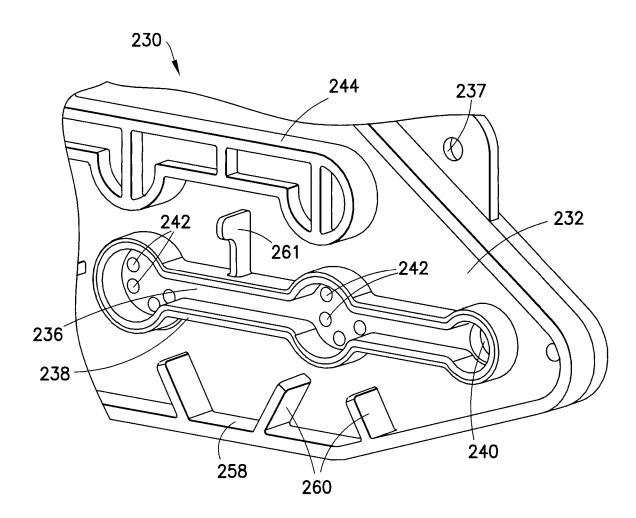
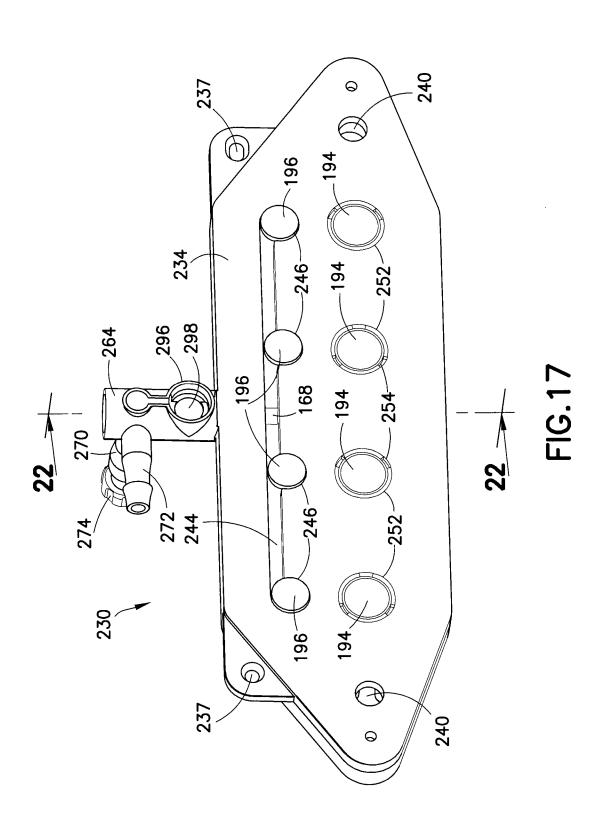


FIG.16

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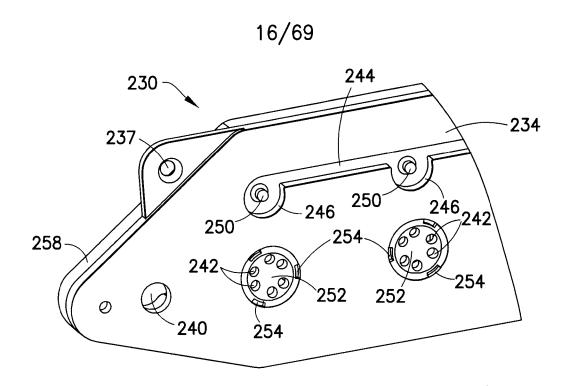


FIG.18

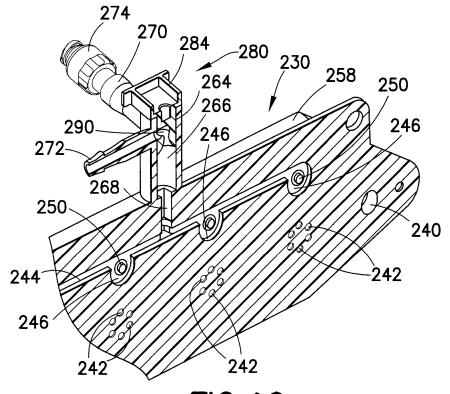


FIG.19

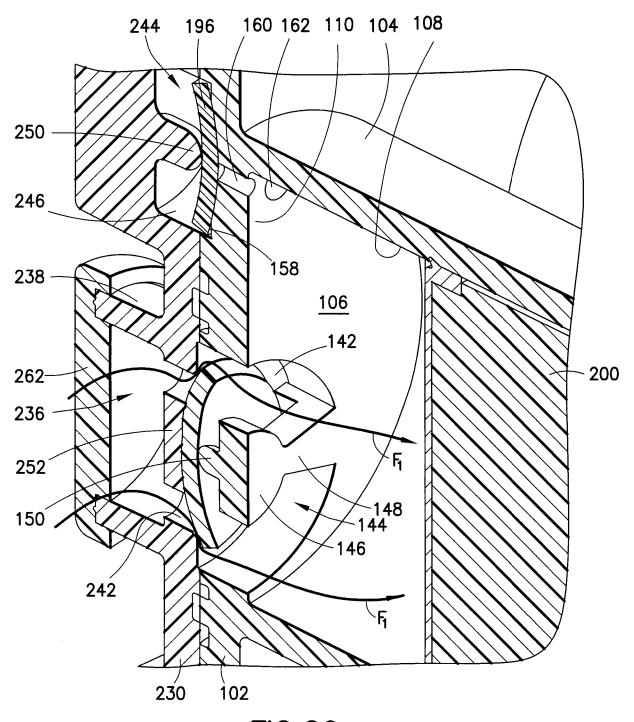
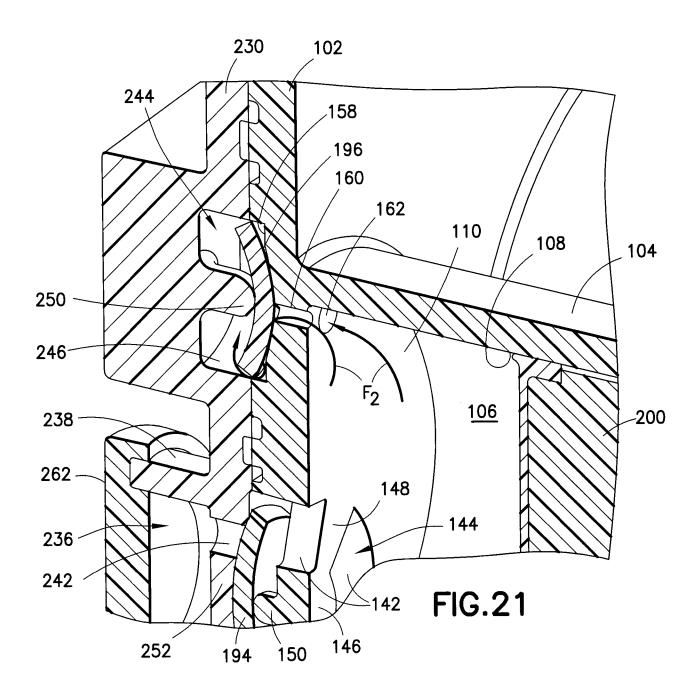


FIG.20



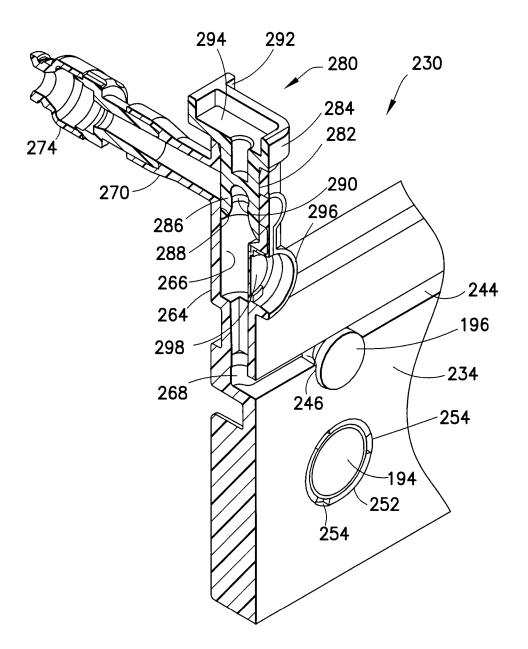
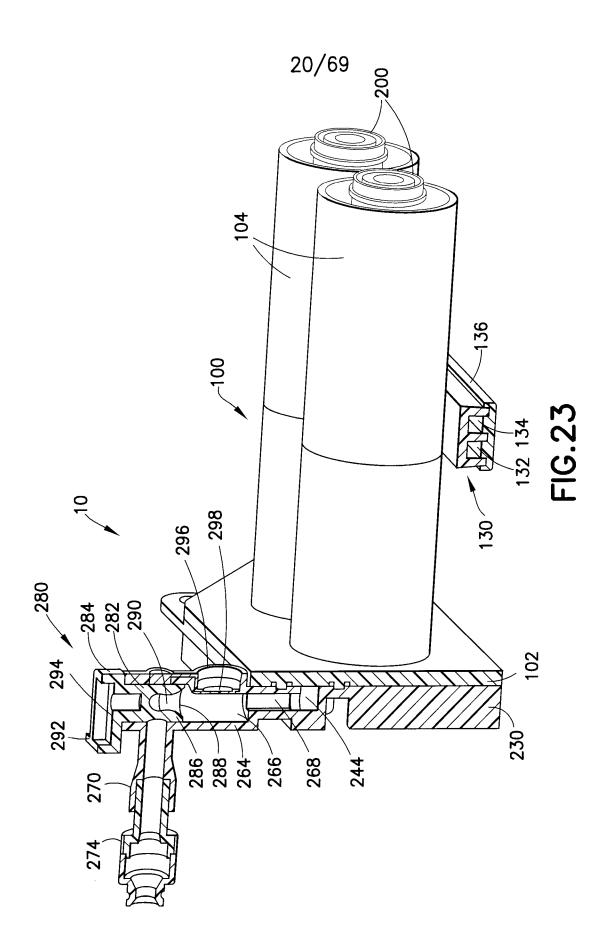
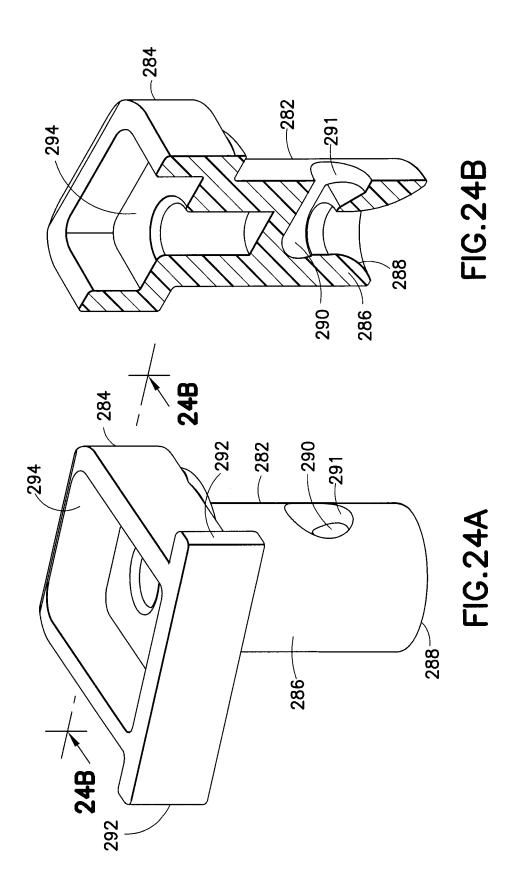
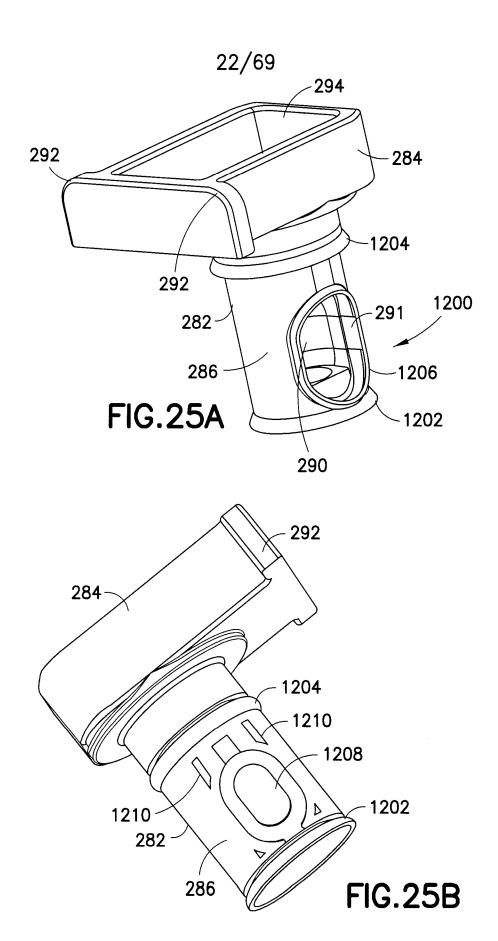


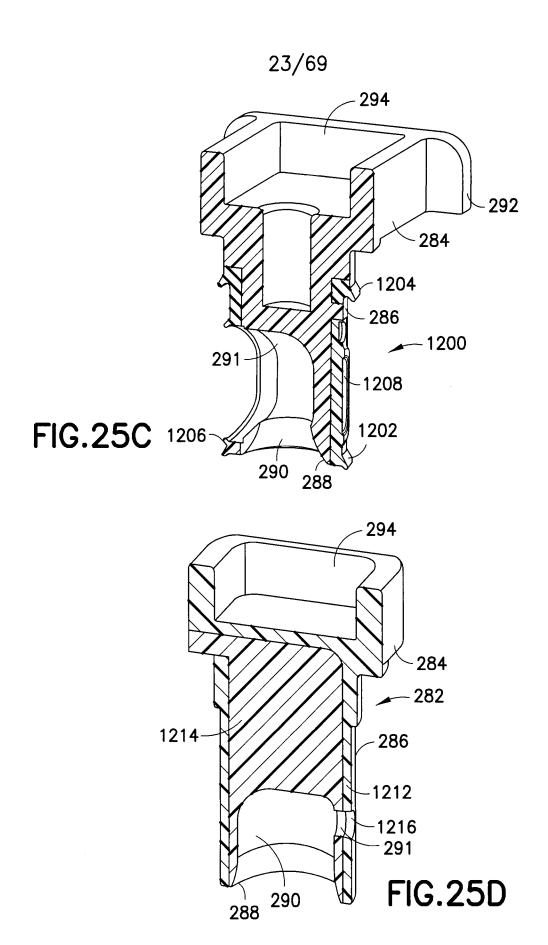
FIG.22

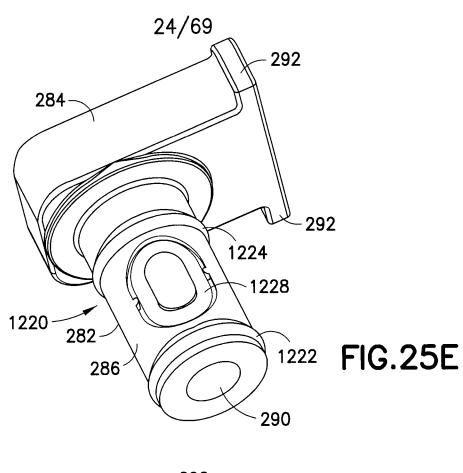


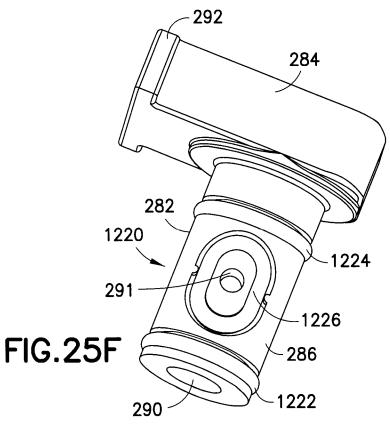


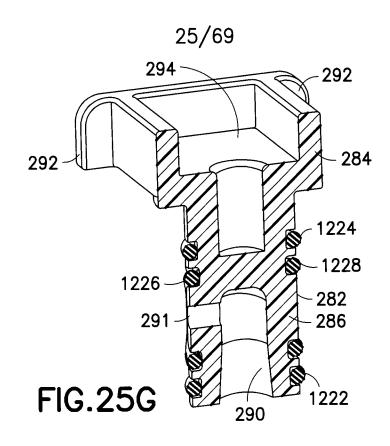












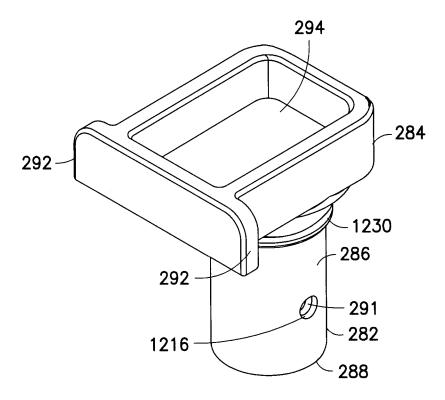


FIG.25H

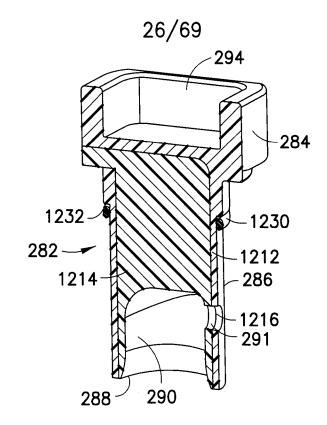
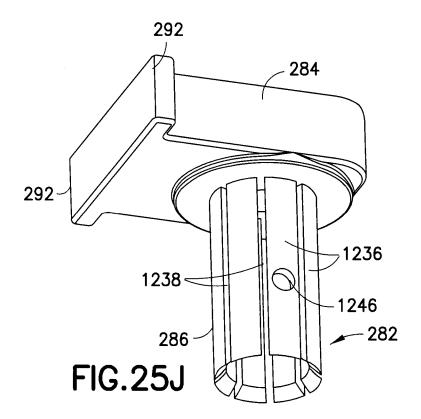


FIG.251



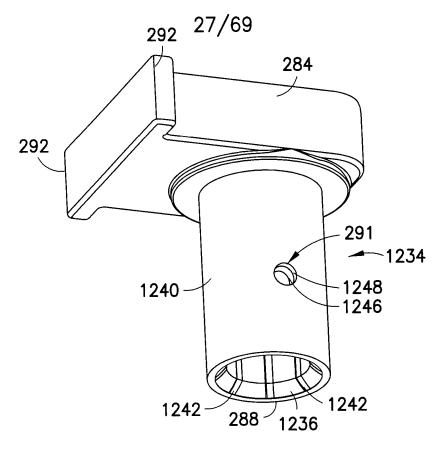


FIG.25K

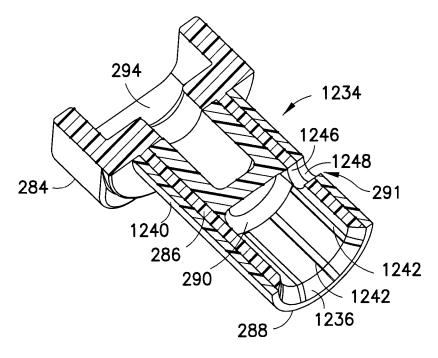
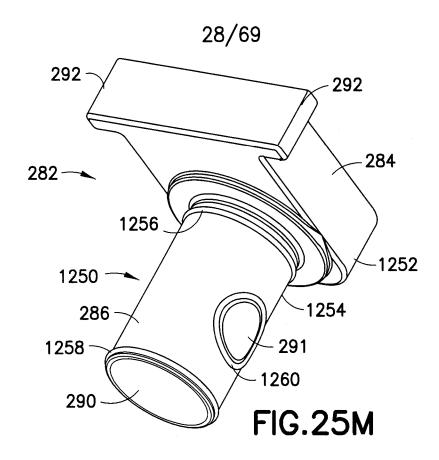
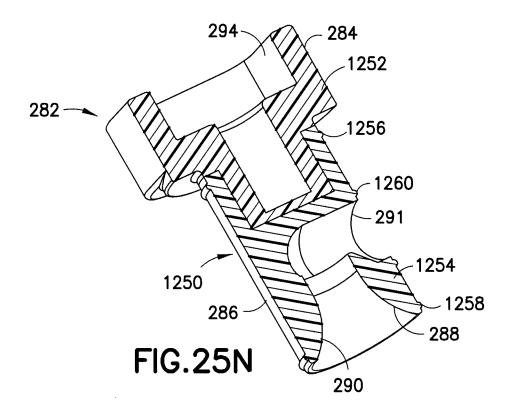
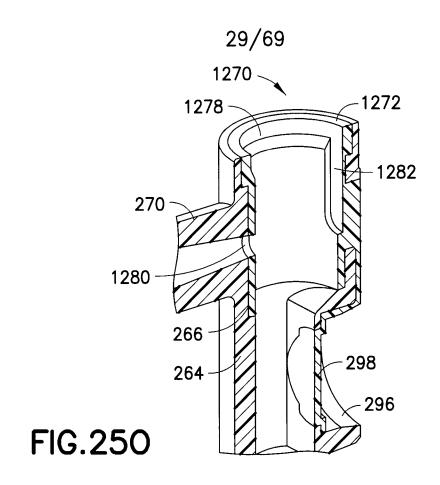
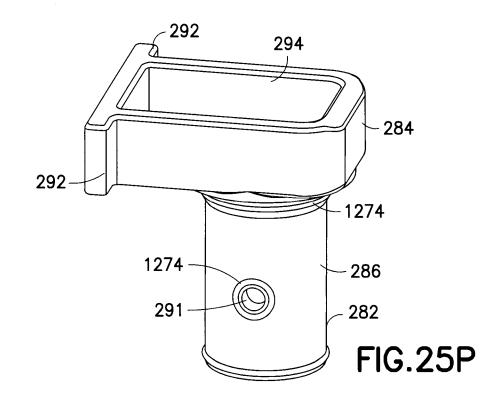


FIG.25L









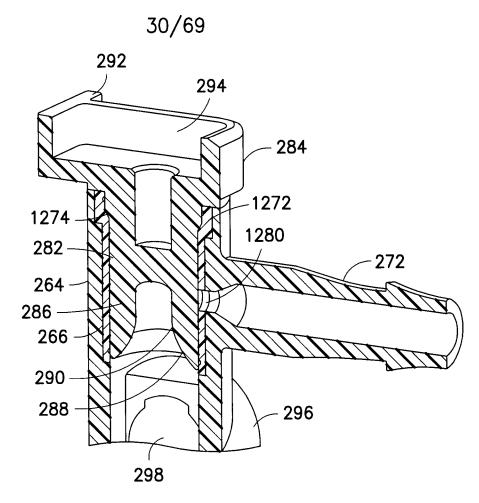


FIG.25Q

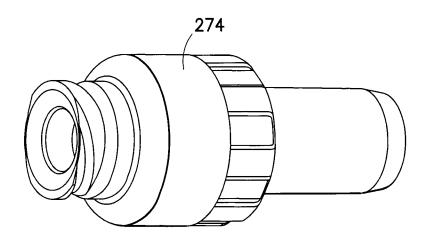
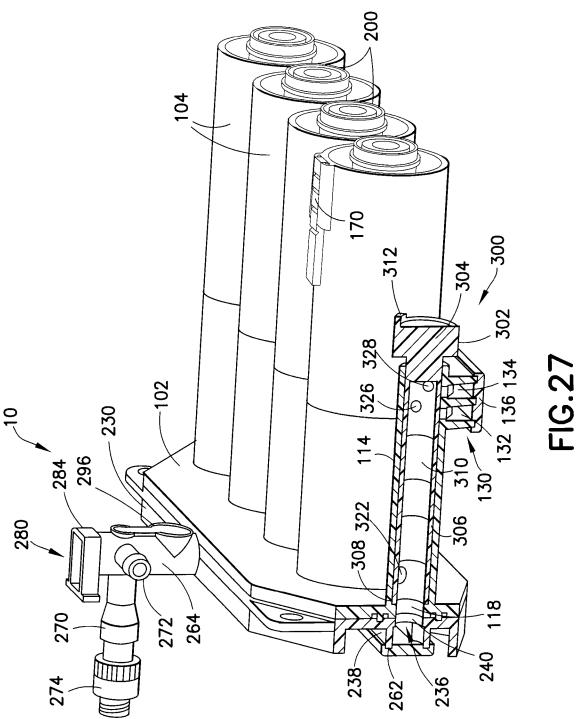
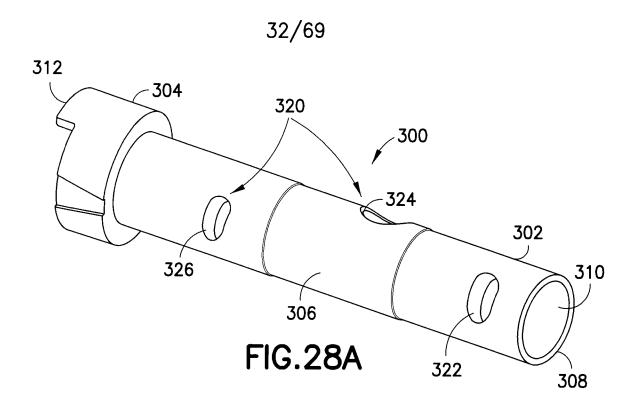


FIG.26







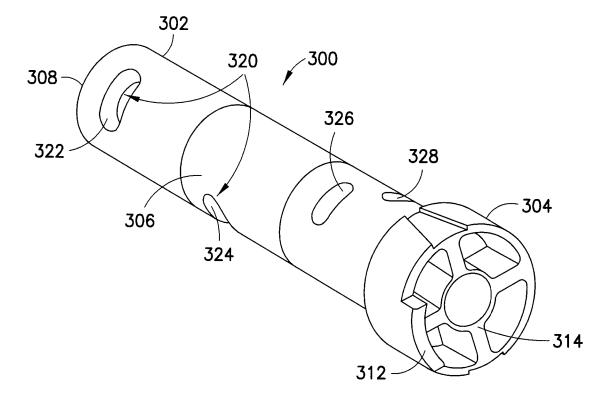
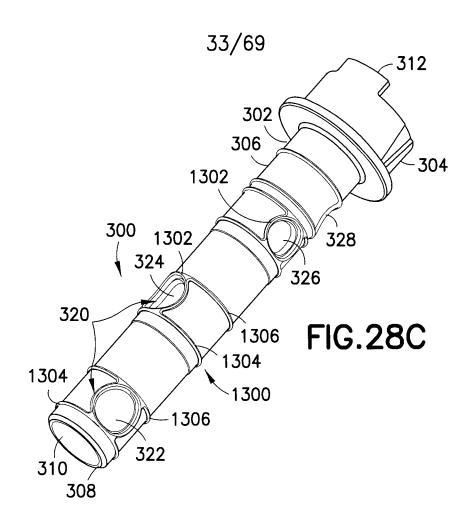
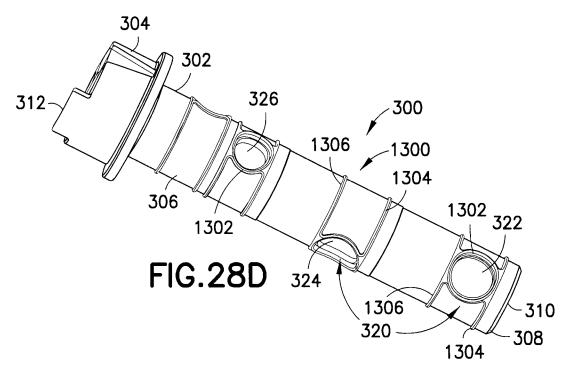
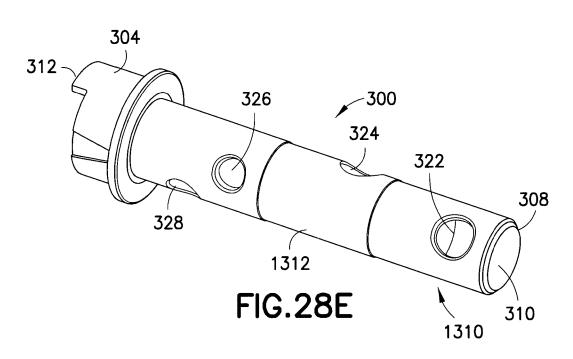


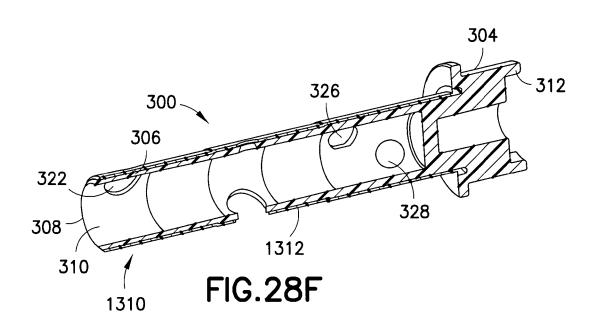
FIG.28B











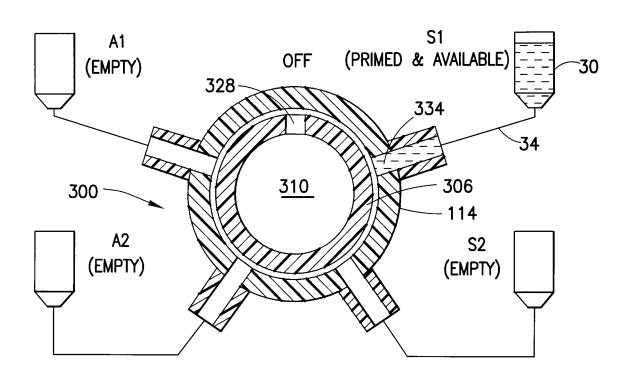


FIG.29A

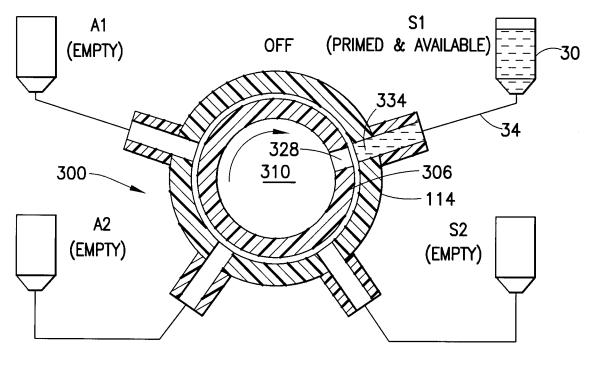
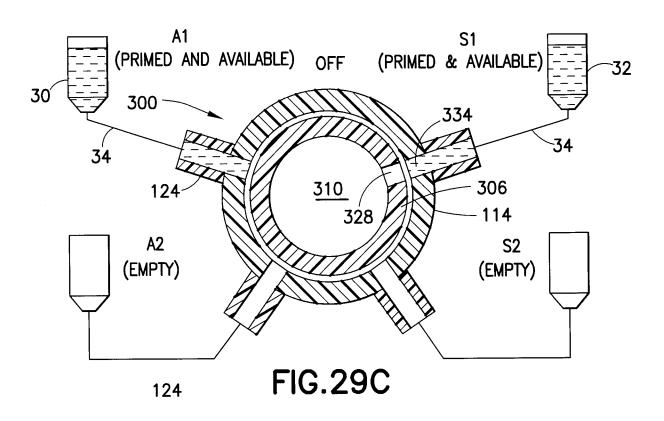
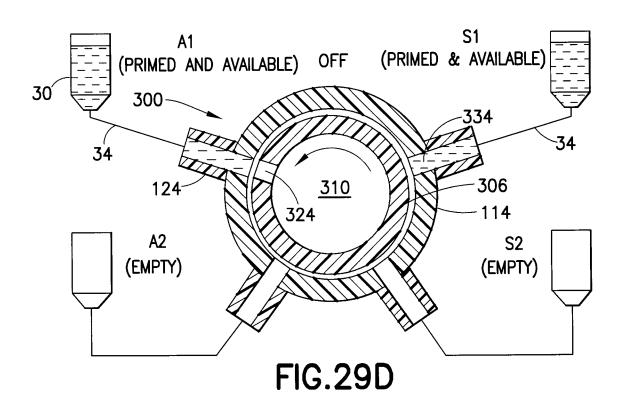


FIG.29B





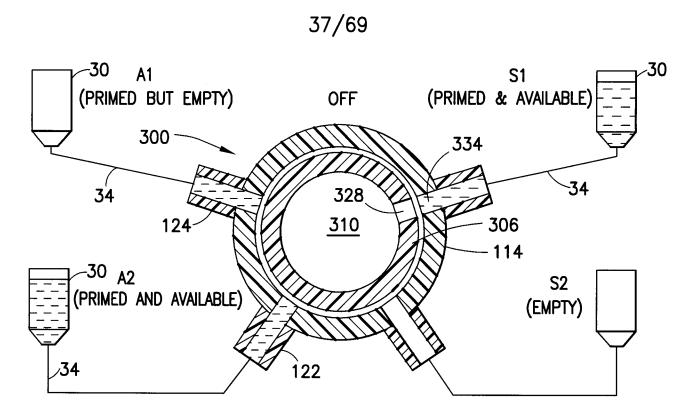
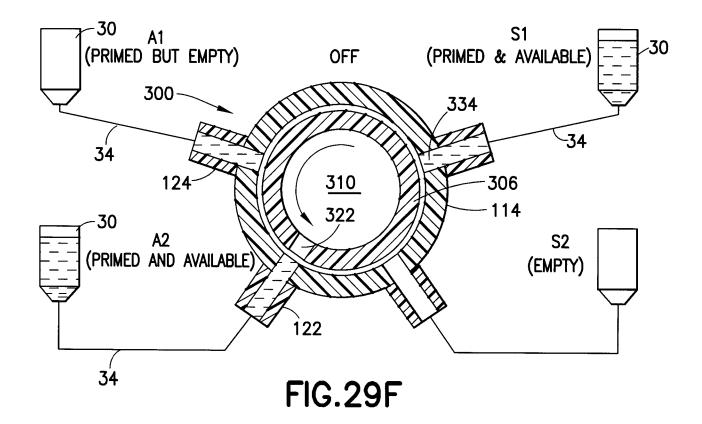
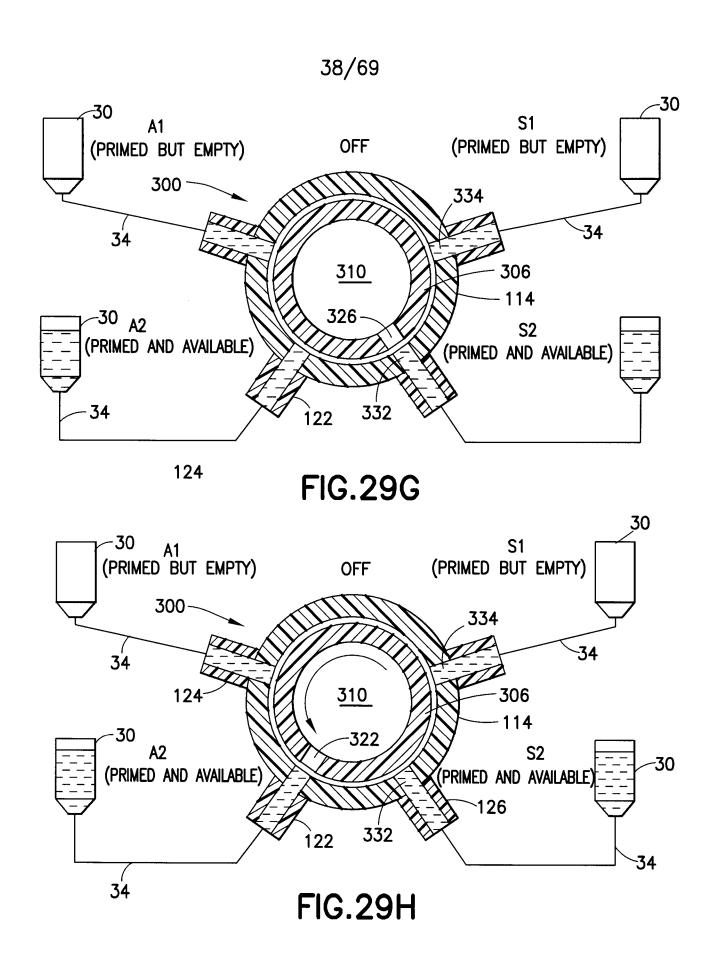
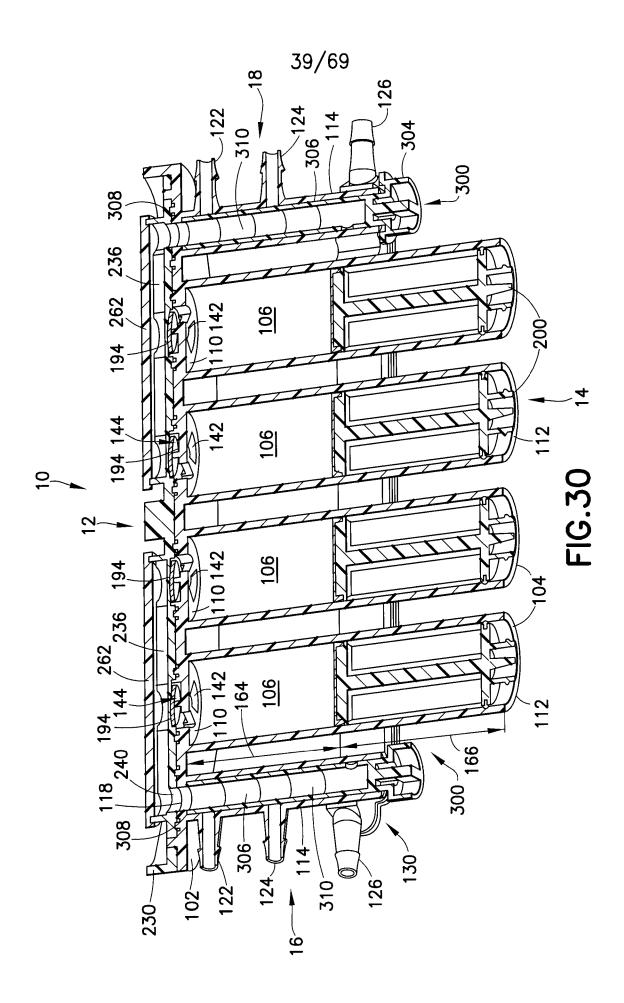


FIG.29E







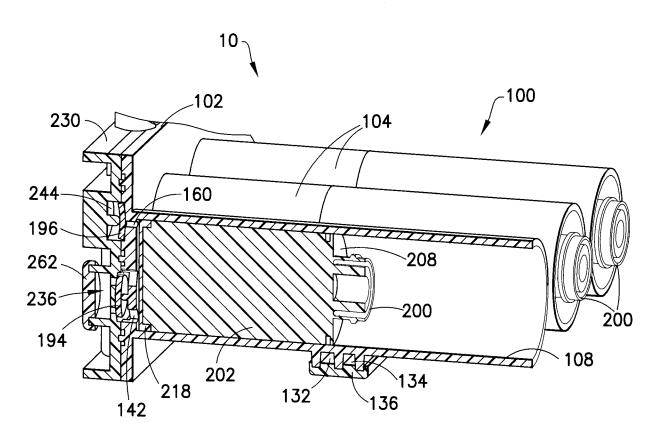
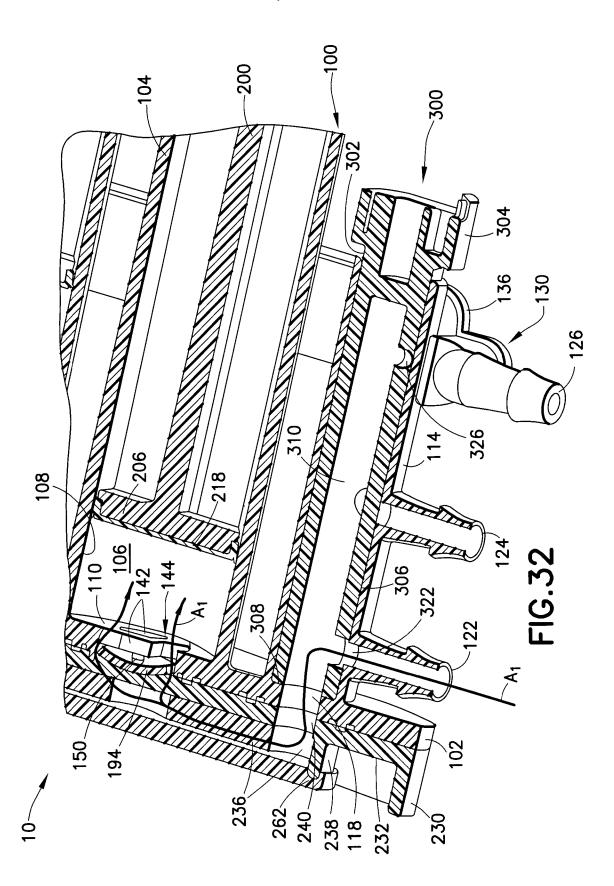
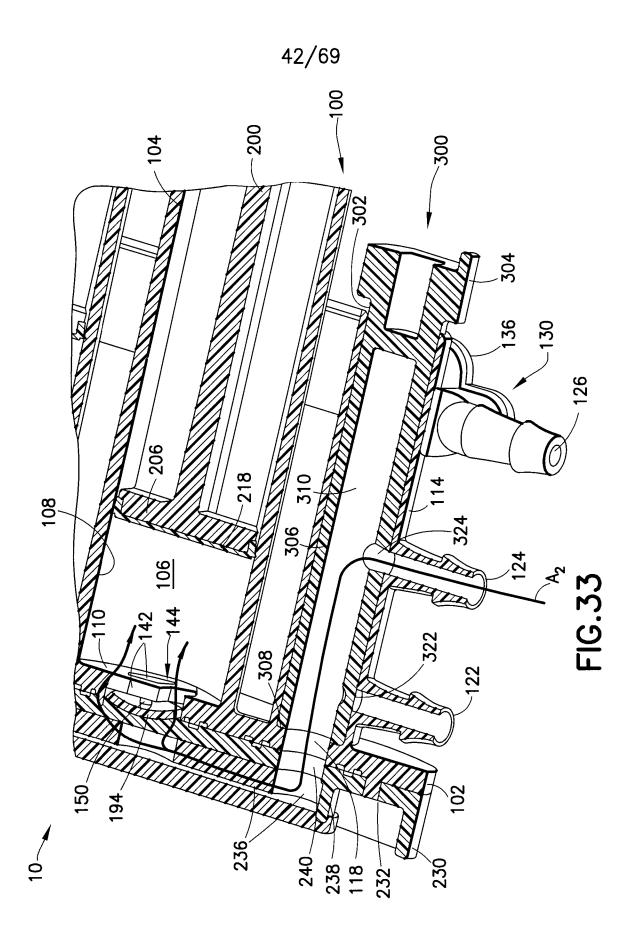
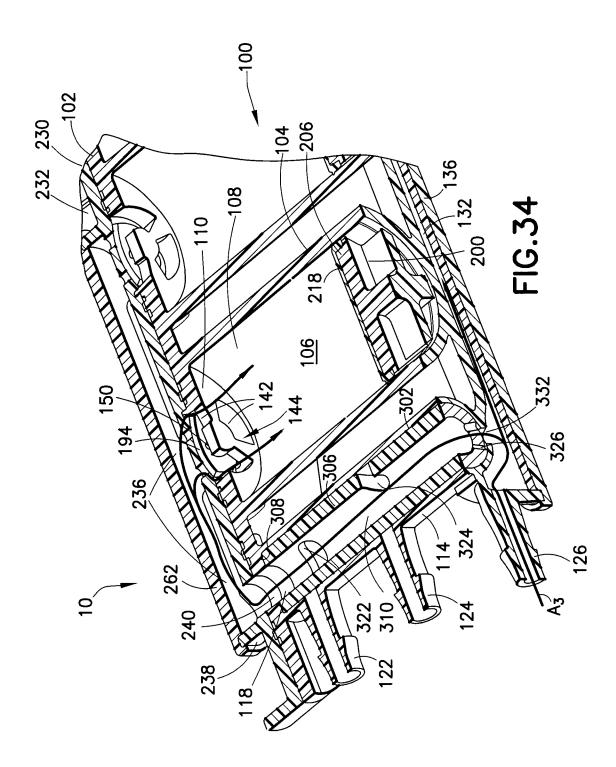


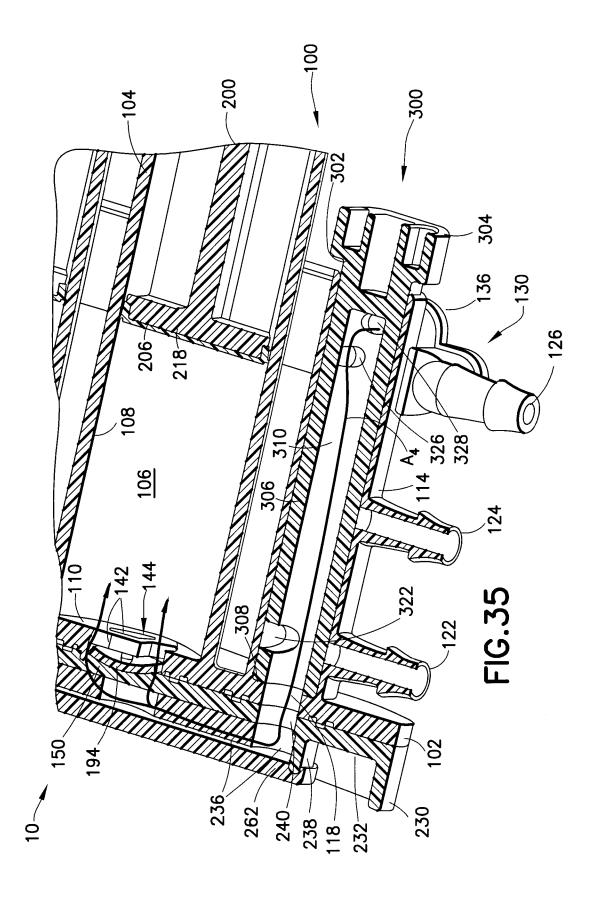
FIG.31

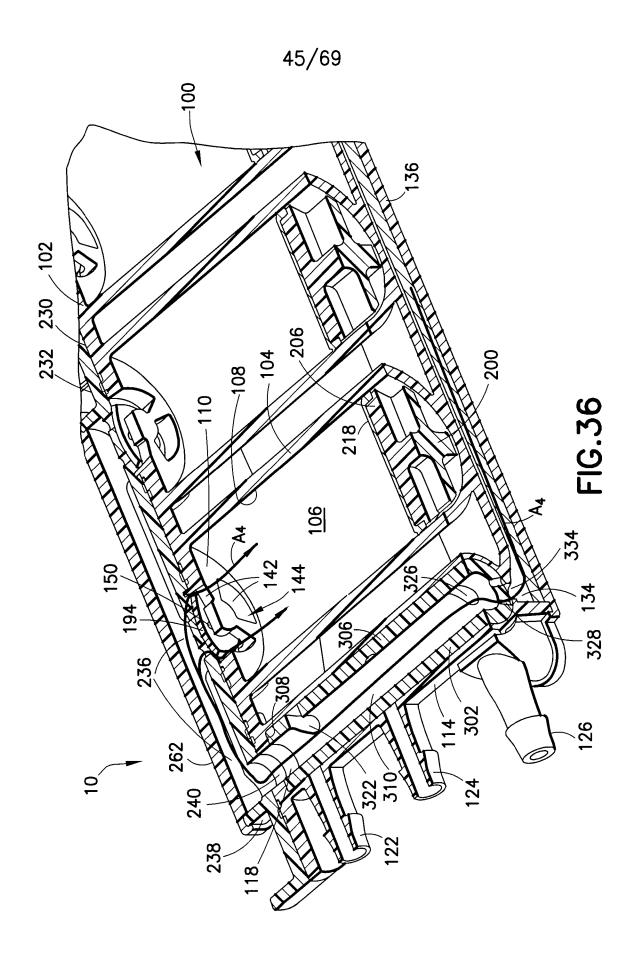


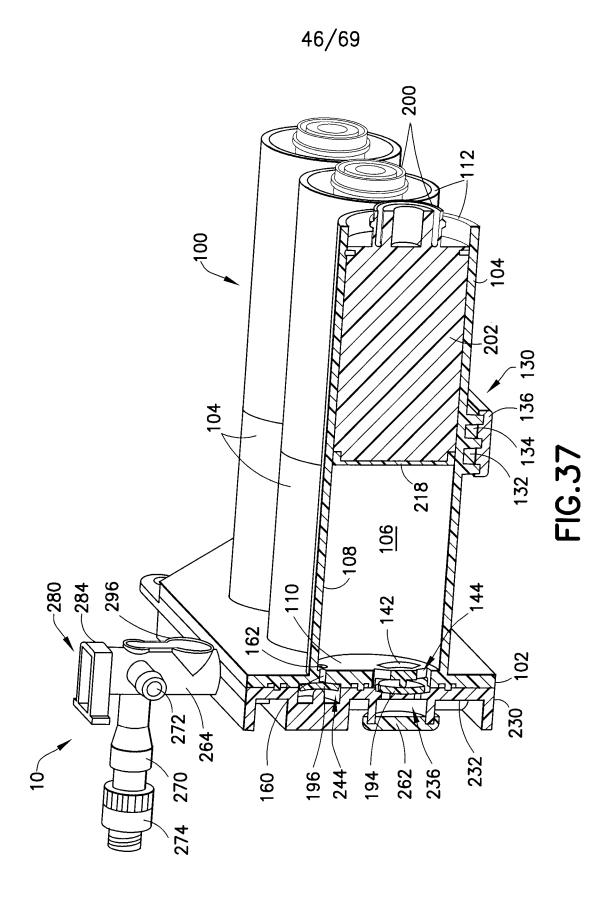












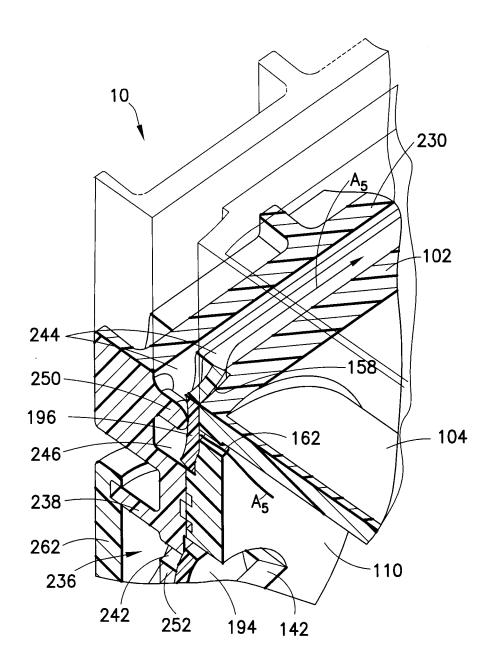


FIG.38

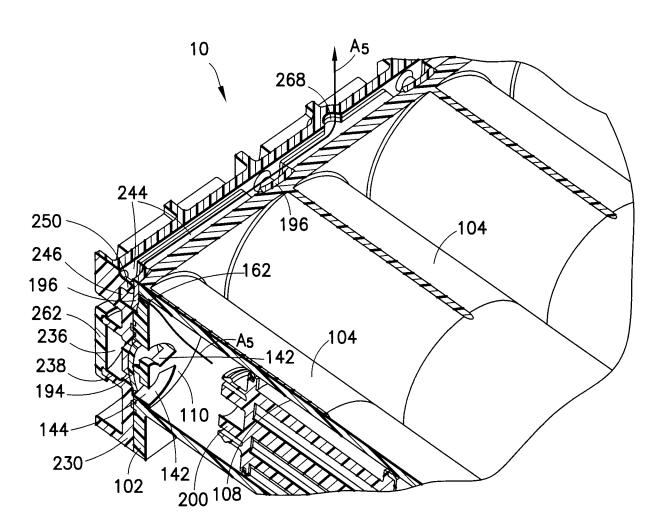
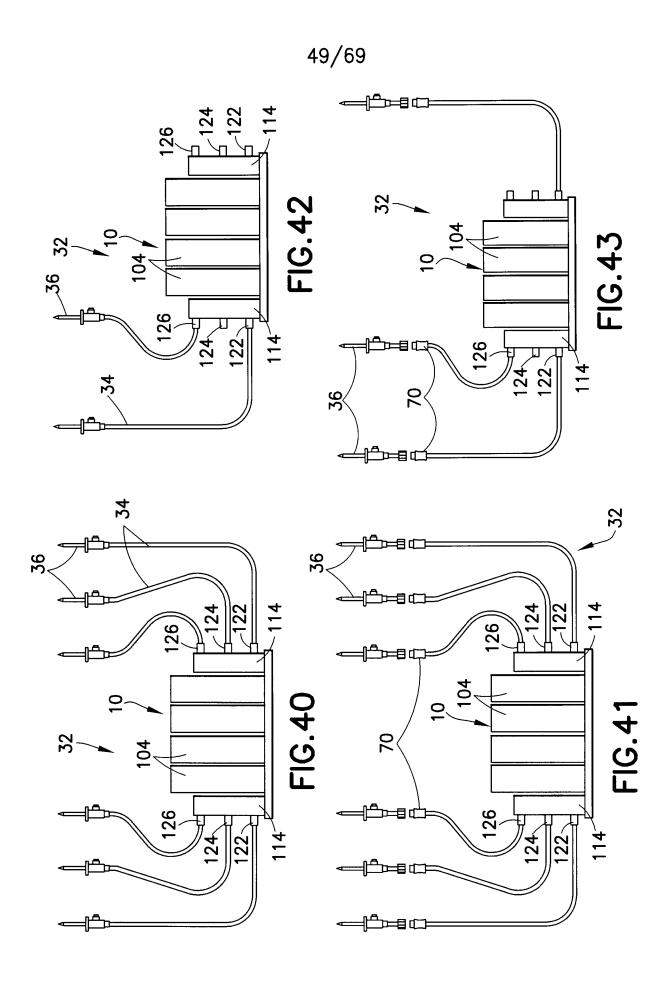
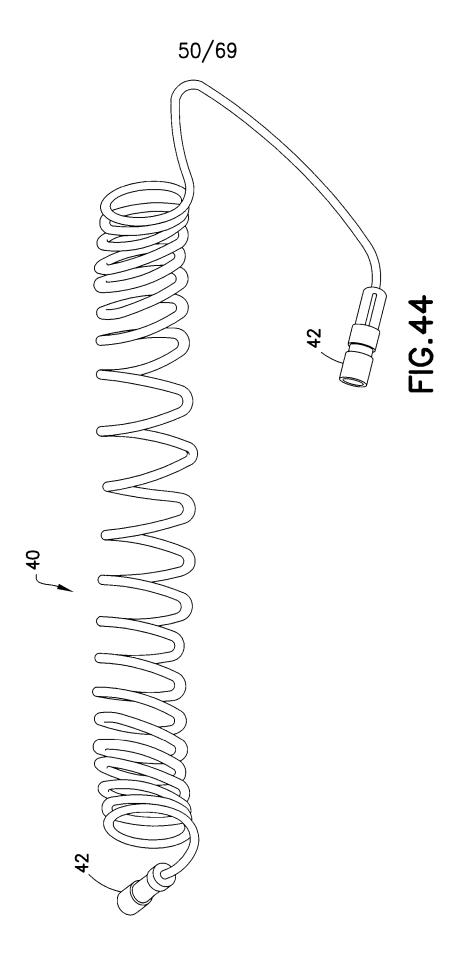
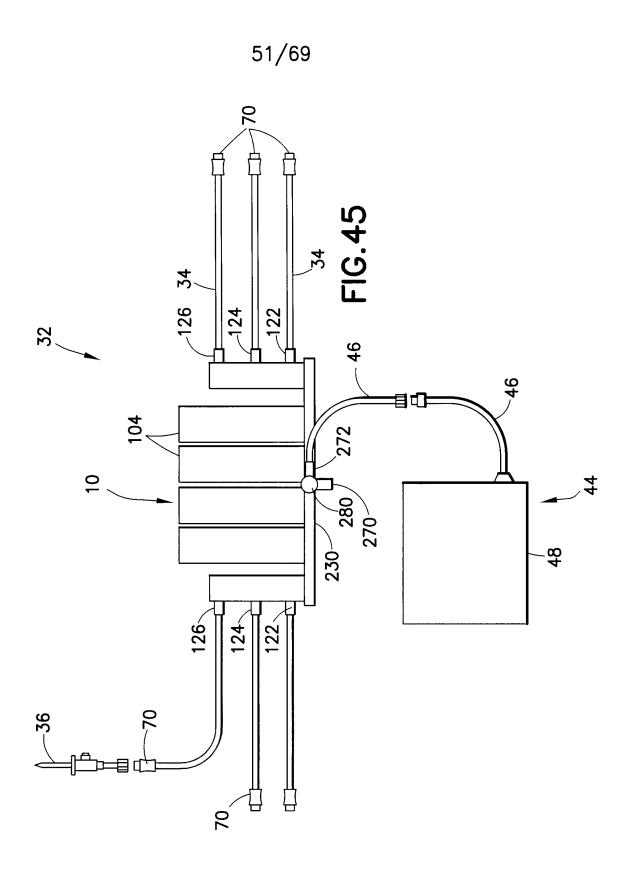
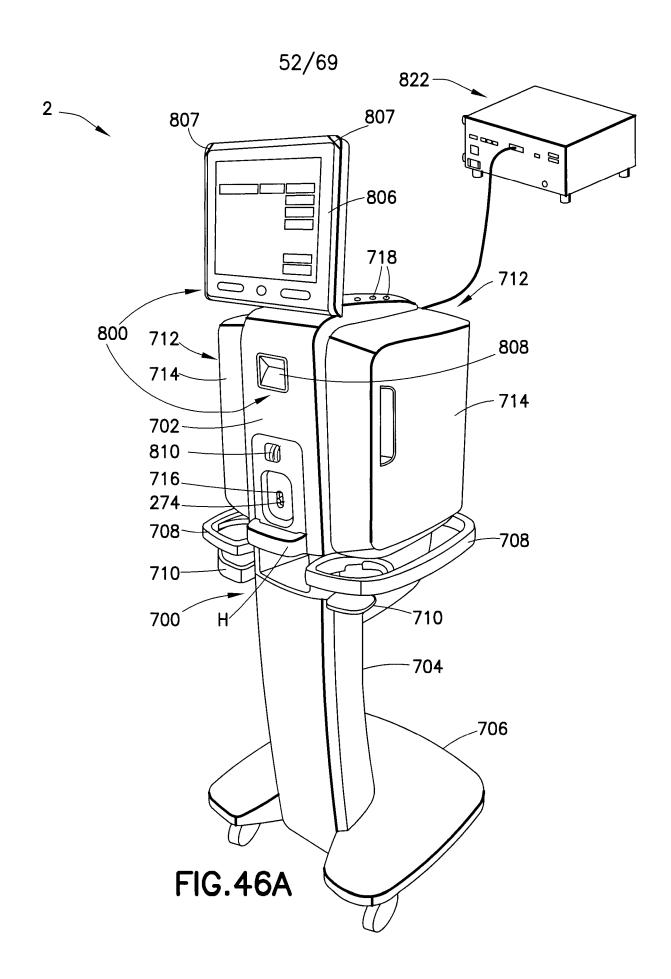


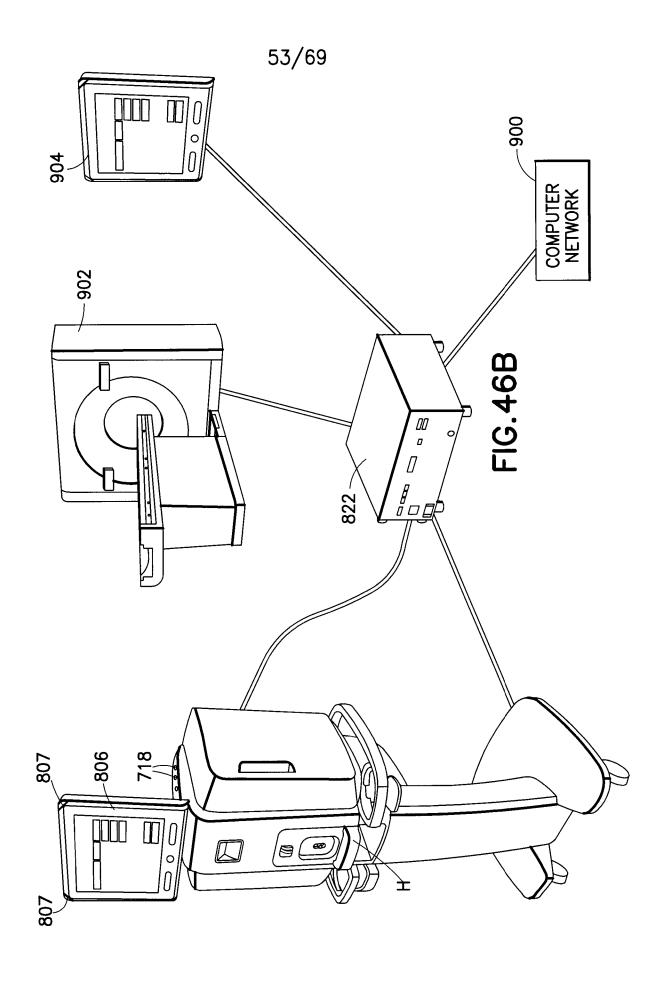
FIG.39











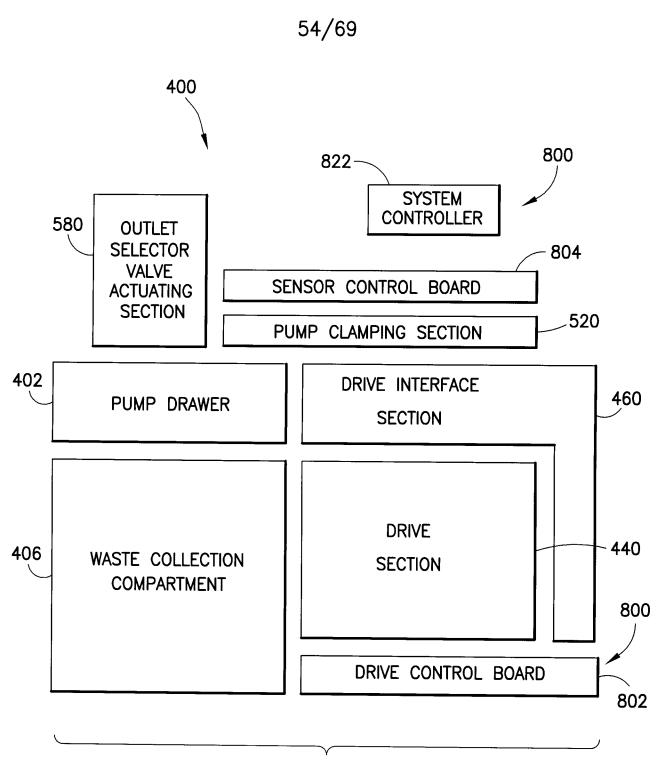


FIG.47

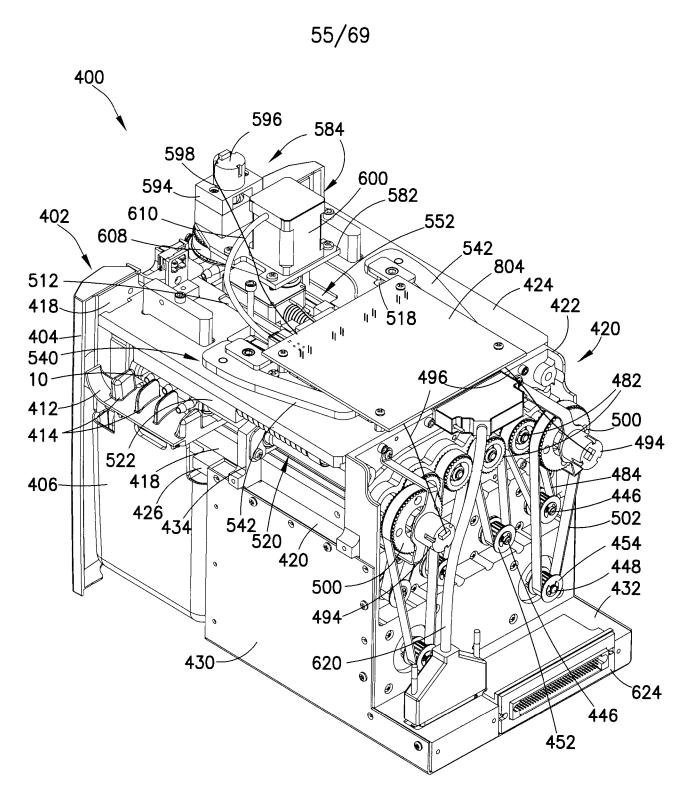
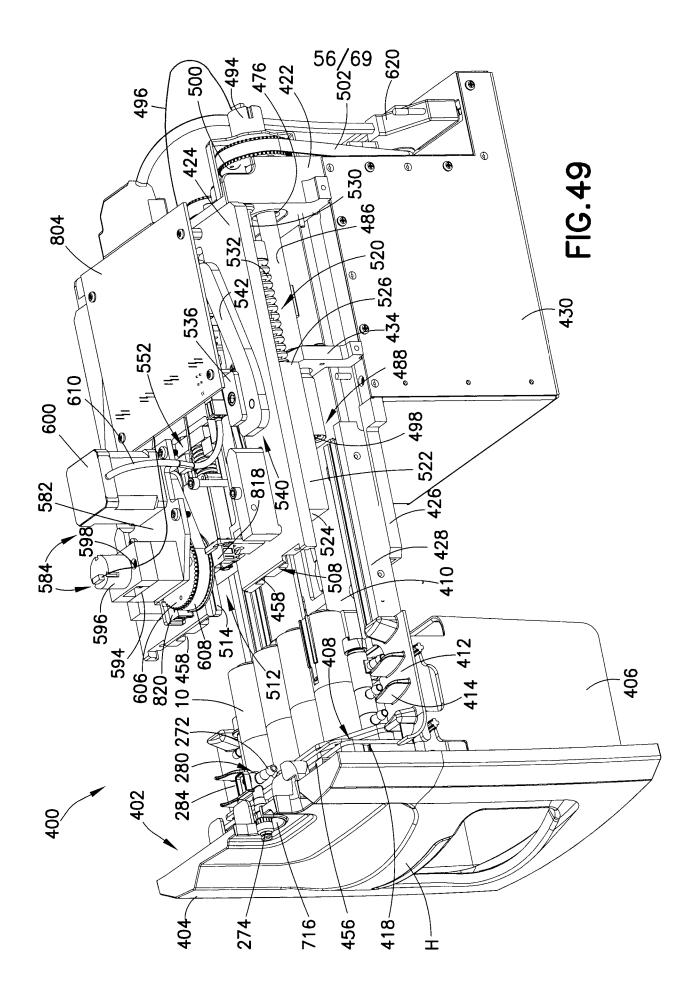
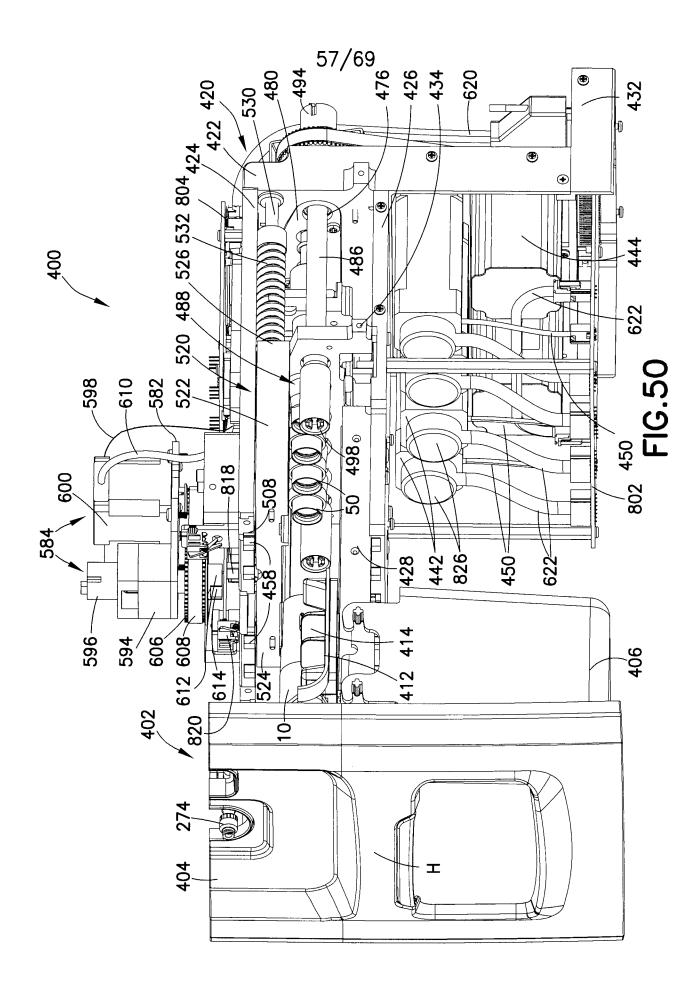
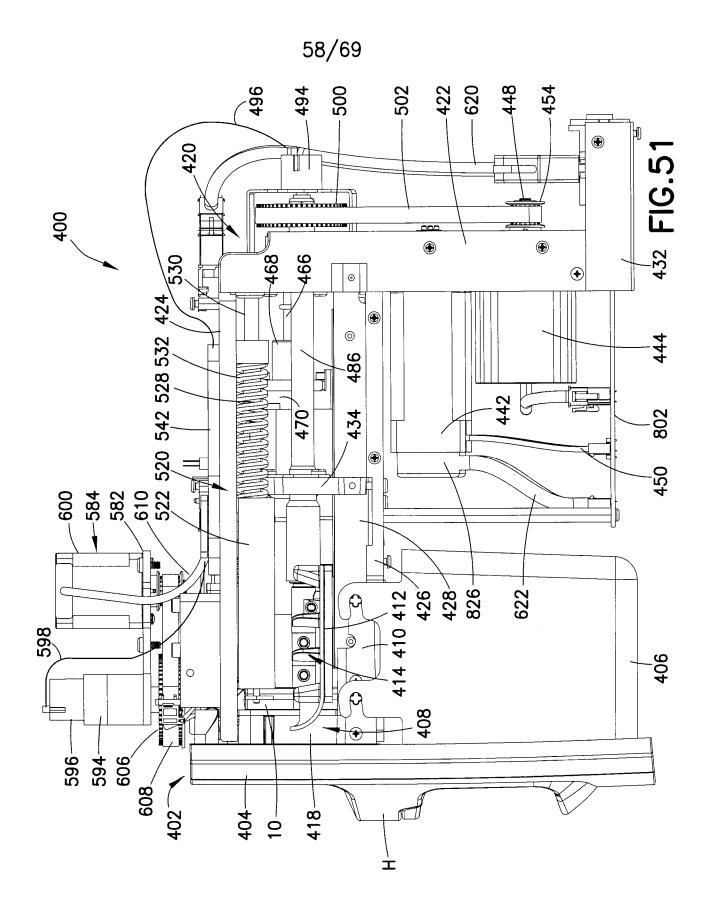
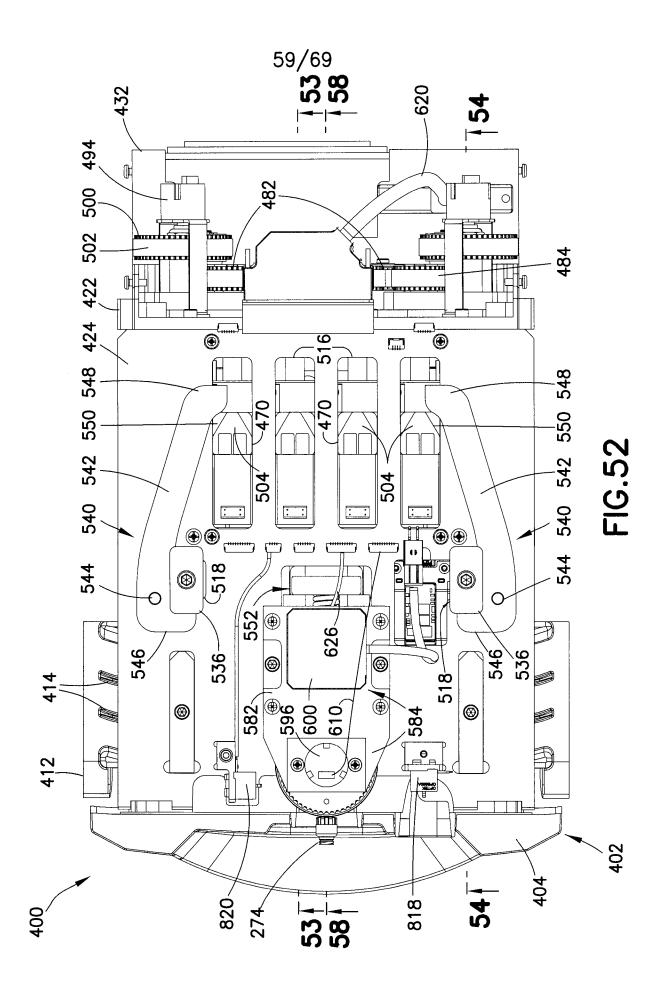


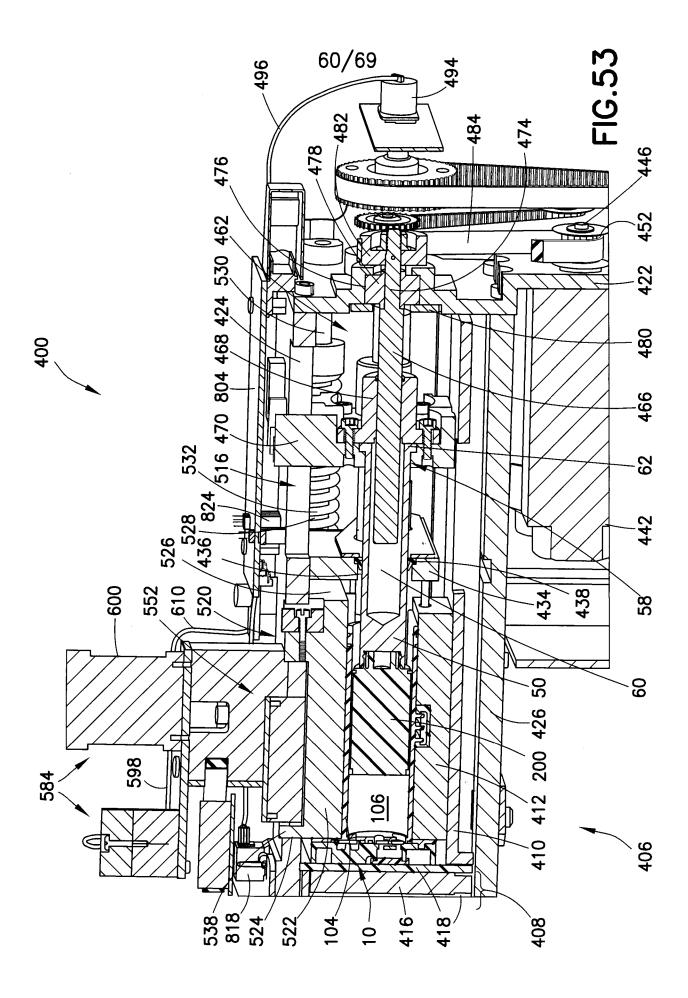
FIG.48

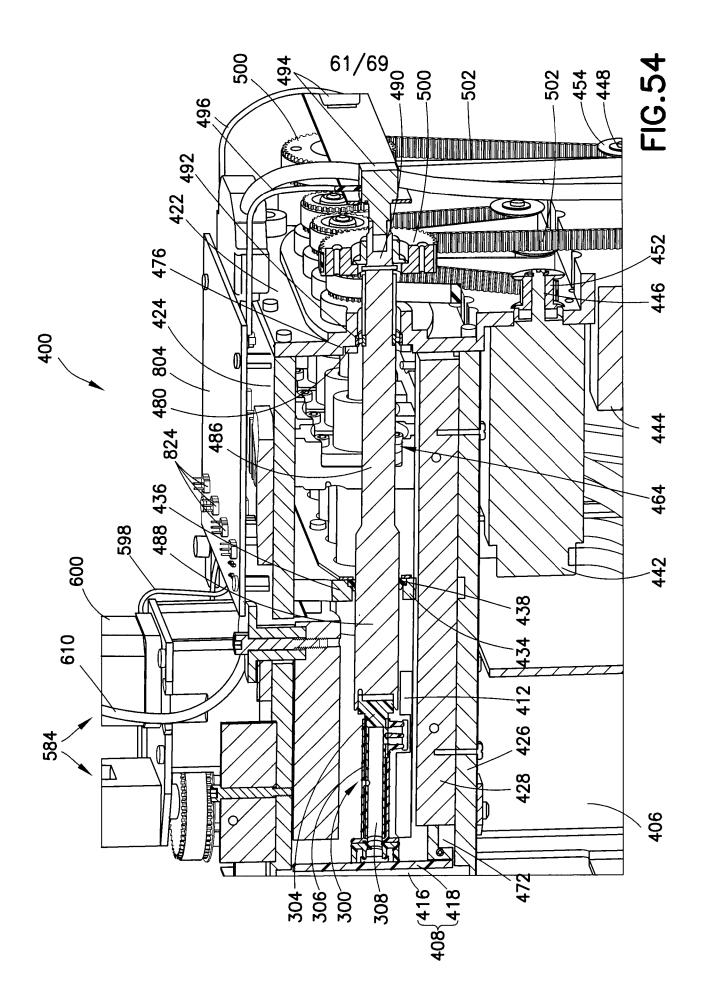


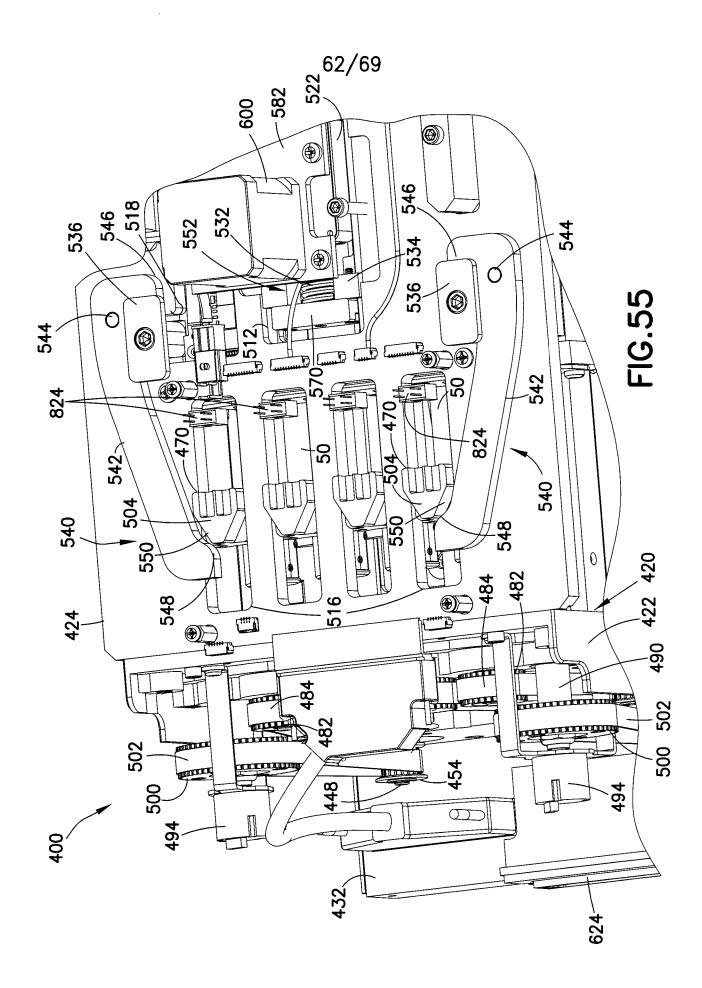


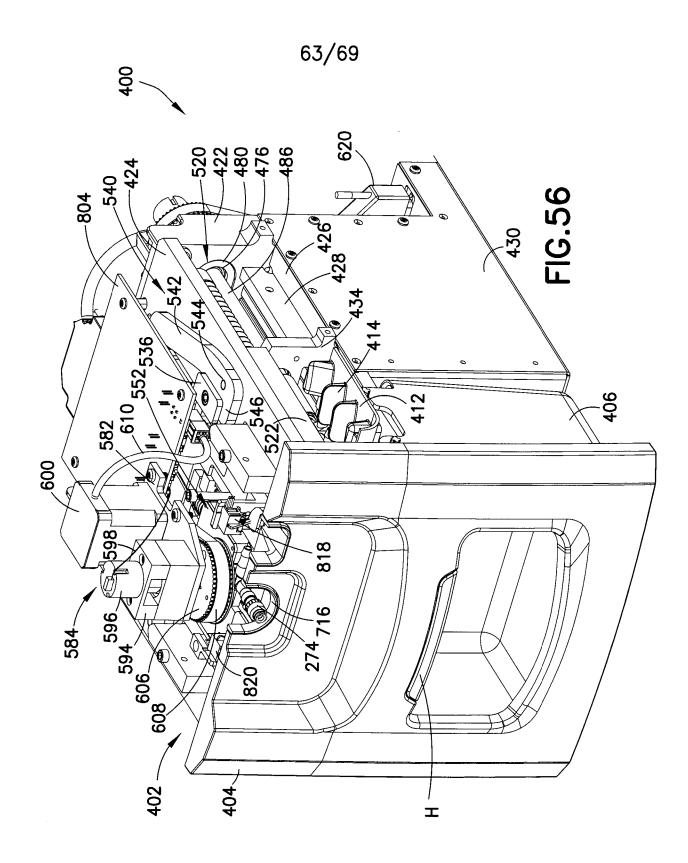


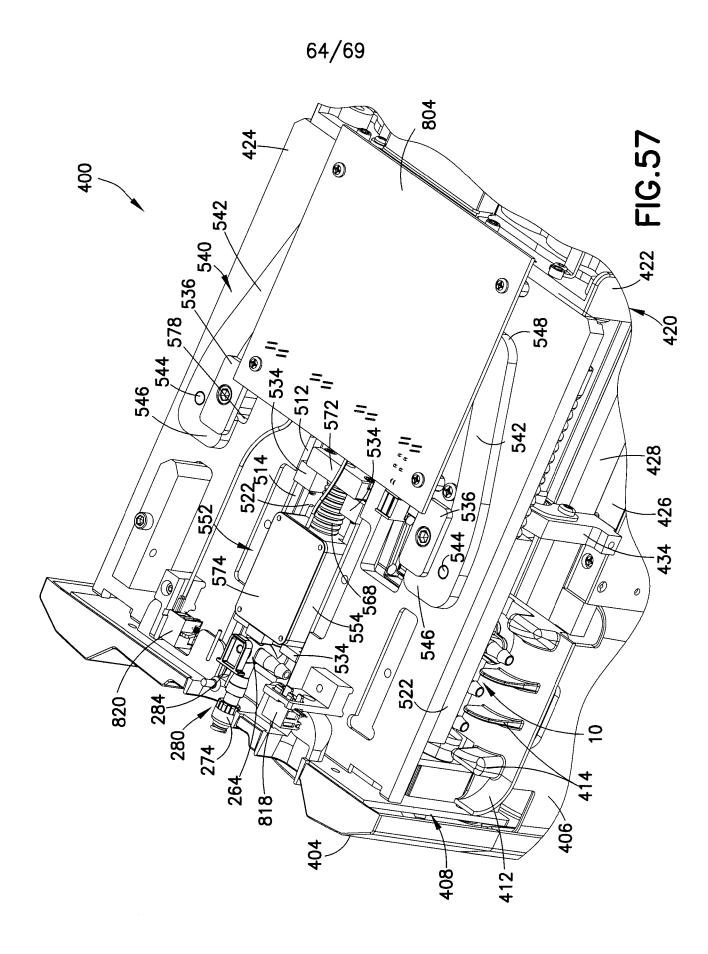


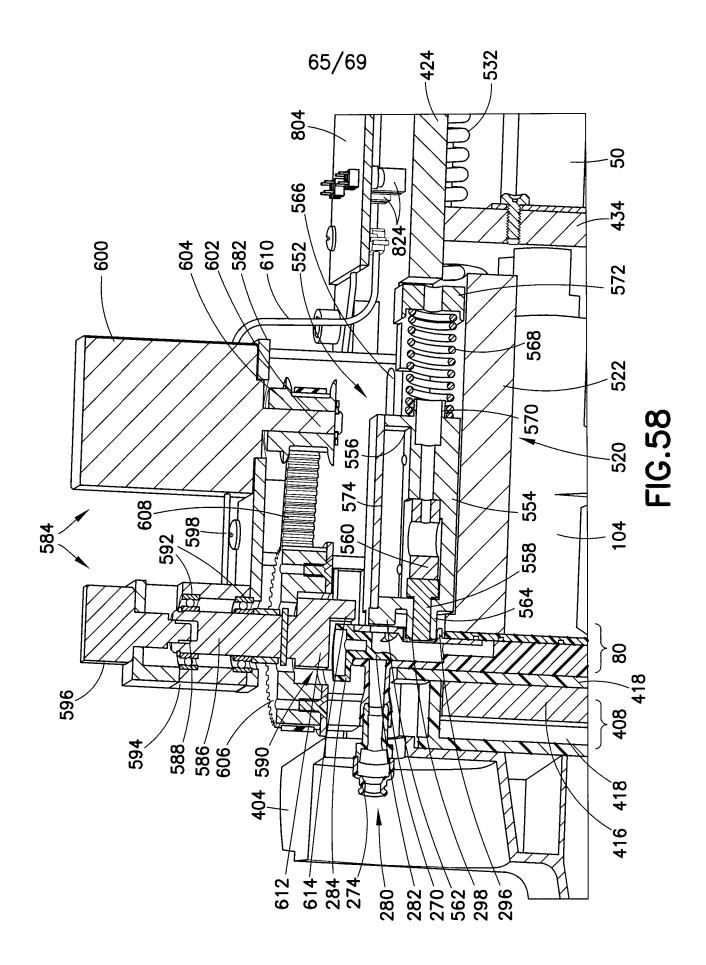


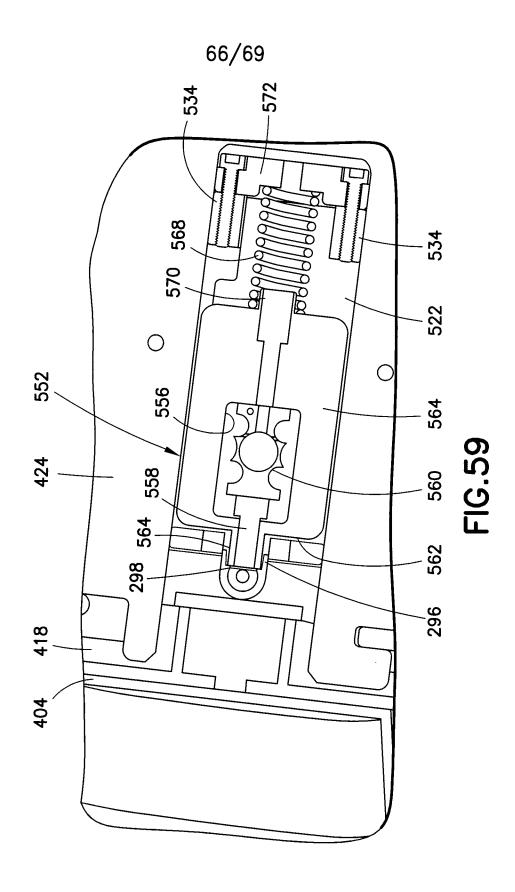












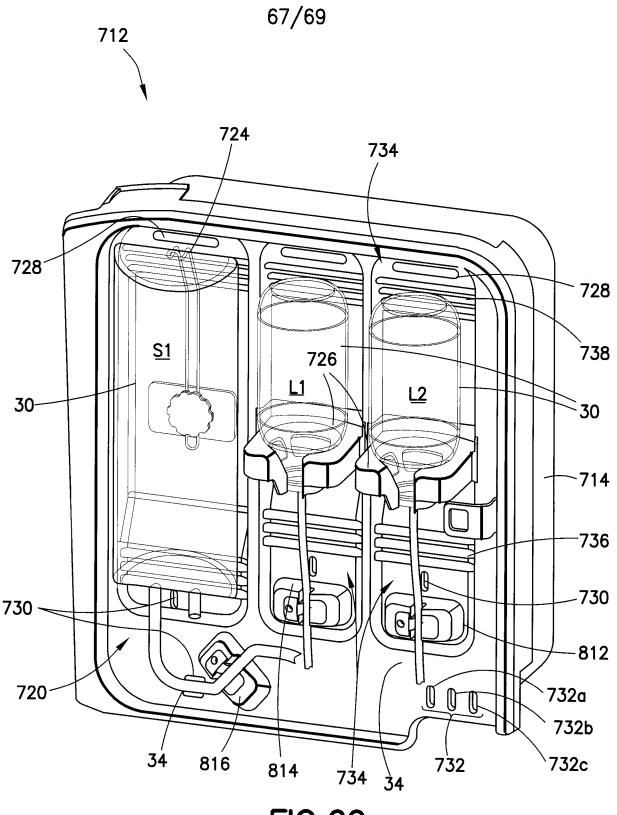
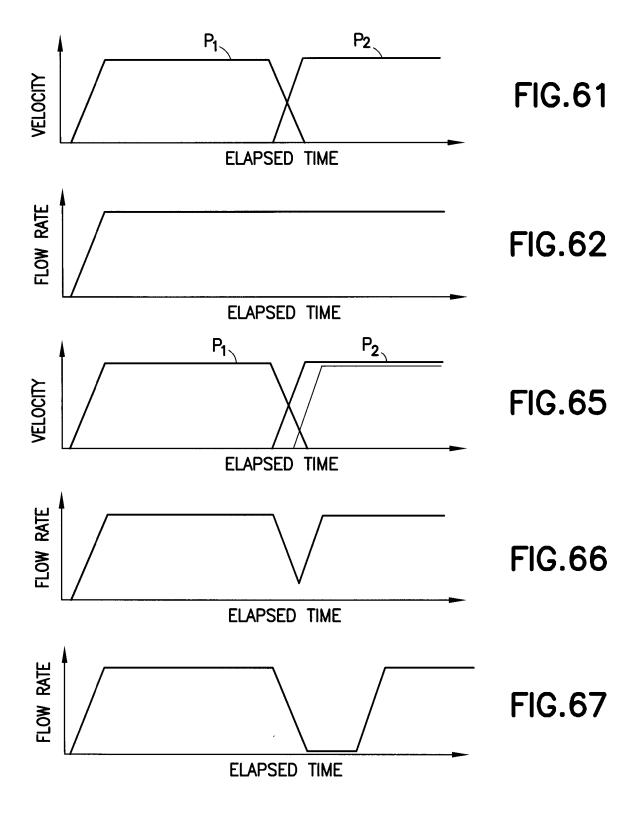
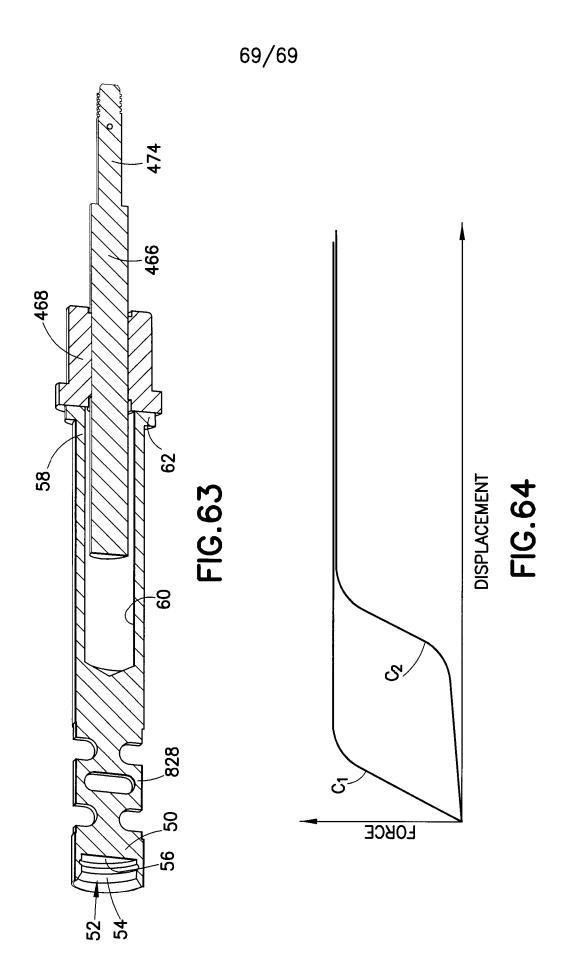


FIG.60







INTERNATIONAL SEARCH REPORT

International application No. PCT/US 12/56328

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IPC(8) - A61M 5/142, 5/145; F04B 15/00, 19/04; F16K 11/02 (2012.01)

USPC - 417/442

According to International Patent Classification (IPC) or to both national classification and IPC

FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols) IPC(8) - A61M 5/142, 145; F04B 15/00, 19/04; F16K 11/02 (2012.01) USPC - 417/442

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched USPC - 137/597, 625, 625.4, 625.42; 417/338, 426, 427, 478, 485, 521, 522, 523, 524, 536, 538 (text search - see terms below)

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used) PubWEST(USPT,PGPB,EPAB,JPAB); PatBase; Google Scholar; Google Patents

Search Terms: select, valve, pump, plunger, manifold, selector, cylinder, indicia, drawer, clamp, piston, disc, radial, lip,... etc.

C. DOCU	MENTS CONSIDERED TO BE RELEVANT		····				
Category*	Citation of document, with indication, where a	Relevant to claim No.					
X	US 2011/0200456 A1 (Patzer) 18 August 2011 (18.08		1-4 and 10-12				
Y	[0060], [0068], [0080]-[0084], [0088] and [0091]-[0092]		5-9 and 13-50				
Y	US 2010/0298699 A1 (Reilly et al.) 25 November 2010	5 and 6					
Y	US 4,469,121 A (Moen) 04 September 1984 (04.09.19	7-9 and 15-17					
Y	US 6,436,072 B1 (Kullas et al.) 20 August 2002 (20.08	13-20					
Y	US 2008/0034959 A1 (Vu) 14 February 2008 (14.02.2	21-50					
Y	US 6,197,000 B1 (Reilly et al.) 06 March 2001 (06.03.	21-26 and 38-50					
Υ	US 5,362,291 A (Williamson, IV) 08 November 1994 (col 6, ln 16-42	27-41					
Y	US 2004/0074281 A1 (Lobdell et al.) 22 April 2004 (22	33-35					
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26 Novemb	er 2012 (26.11.2012)	1 3 DEC 2012					
	nailing address of the ISA/US	Authorized officer:					
	T, Attn: ISA/US, Commissioner for Patents 50, Alexandria, Virginia 22313-1450	Lee W. Young					
	0. 571-273-3201	PCT Helpdesk: 571-272-4300 PCT OSP: 571-272-7774					