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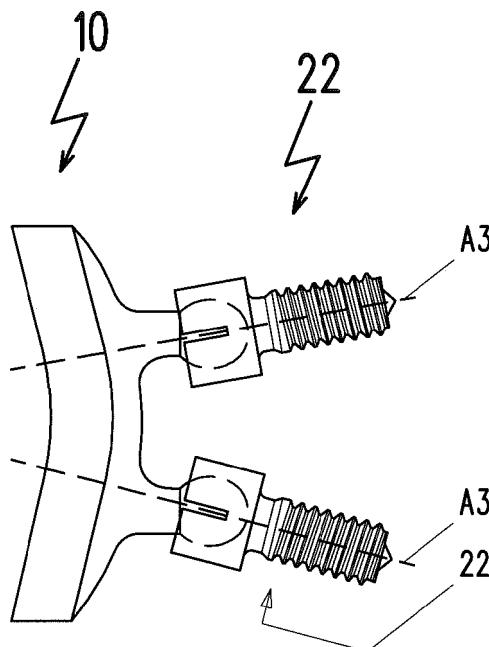
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(54) Title: A SET FOR CONNECTING A PROSTHETIC ASSEMBLY OF AN ARTIFICIAL JOINT TO A BONE



(57) Abstract: The present disclosure relates to a set for connecting a prosthetic assembly of an artificial joint, in particular a glenoidal component of a shoulder prosthesis, to a bone, the set comprising: - a prosthetic component comprising a bone contacting surface contacting the bone in an implanted state of the prosthetic component and - separate bone anchoring means, wherein the bone contacting surface of the prosthetic component is provided with a coupling means adapted to be coupled to the bone anchoring means in a mounted state of the prosthetic component. The coupling means and the bone anchoring means are adapted to achieve a tight-fit connection or a form-fit connection, in particular a snap-fit connection, with each other.

Fig. 3a

**A SET FOR CONNECTING A PROSTHETIC ASSEMBLY
OF AN ARTIFICIAL JOINT TO A BONE**

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The present disclosure relates to a set for connecting a prosthetic assembly of an artificial joint to a bone.

E.g. document WO 2007/057054 A discloses a set of the aforementioned kind.

The articulation surface of natural joints can be damaged by wear or injuries to

10 such a degree that a prosthetic component has to replace the damaged natural component of the joint. E.g. in cases of shoulder joint arthritis, where the glenoid has been compromised by articular damage, and in particular the rotator cuff is repairable or intact, the current state of the art is to install a cemented glenoid prosthesis. Cemented glenoid prostheses, however, in some cases suffer due to

15 fixation failures generated via tensile loading incurred by humeral head translation across the glenoid articulation surface. Similar or analog situations and problems are encountered in other joints. Therefore, there is a need for an improved concept to connect a prosthetic component of an artificial joint to a bone that allows an easy yet reliable implantation and fixation of said component.

20 The following discussion of the background to the invention is intended to facilitate an understanding of the invention. However, it should be appreciated that the discussion is not an acknowledgement or admission that any aspect of the discussion was part of the common general knowledge as at the priority date of the application.

25 Where any or all of the terms "comprise", "comprises", "comprised" or "comprising" are used in this specification (including the claims) they are to be interpreted as specifying the presence of the stated features, integers, steps or components, but not precluding the presence of one or more other features, integers, steps or components.

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SUMMARY OF INVENTION

According to the present invention, there is provided a set for connecting a prosthetic assembly of an artificial shoulder joint to a bone, the set comprising: - a glenoidal component comprising a bone contacting surface adapted for contacting the bone in an implanted state of the glenoidal component and an opposed

5 articular surface adapted for contacting an articular surface of a humeral component or a bearing component; and - a separate bone anchoring member extending along a first longitudinal axis, wherein the bone contacting surface of the glenoidal component is provided with a coupling member extending along a second longitudinal axis and adapted to be coupled to the bone anchoring

10 member in the implanted state of the glenoidal component, and wherein the coupling member and the bone anchoring member are adapted to achieve a tight-fit connection with each other; - the coupling member comprising a peg extending from the bone contacting surface of the glenoidal component and an essentially spherical ball head disposed at an end of the peg, the peg having a smaller cross-section than the ball head in a plane perpendicular to the second longitudinal axis of the coupling member; and - the anchoring member comprising a threaded shaft adapted for insertion into the bone and a head portion including a partially spherical cavity sized and shaped to receive the ball head, the head portion defining a cavity opening at a distal end of the anchoring member, the cavity

15 shaped to define a portion of a sphere truncated at the cavity opening, wherein a height of the cavity defined between the cavity opening and an opposing bottom surface of the cavity is less than a diameter of the ball head such that a portion of the ball head remains exposed when the coupling member and the anchoring member are attached; - wherein the ball head of the coupling member and the

20 cavity in the head portion of the anchoring member are structured such that, in the implanted state of the glenoidal component, the first longitudinal axis of the anchoring member diverges from the second longitudinal axis of the coupling member such that the first and second longitudinal axes are noncoaxial and nonparallel.

25

30 According to the present invention, there is also provided a set for connecting a prosthetic assembly of an artificial shoulder joint to a bone, the set comprising: - a glenoidal component comprising a bone contacting surface adapted for contacting

the bone in an implanted state of the glenoidal component and an opposed articular surface adapted for contacting an articular surface of a humeral component or a bearing component; and - a separate bone anchoring member extending along a first longitudinal axis, wherein the bone contacting surface of the 5 glenoidal component is provided with a coupling member extending along a second longitudinal axis and adapted to be coupled to the bone anchoring member in the implanted state of the glenoidal component, and wherein the coupling member and the bone anchoring member are adapted to achieve a snap-fit connection with each other; the coupling member comprising a peg extending 10 from the bone contacting surface of the glenoidal component and a ball head disposed at an end of the peg, the peg having a smaller cross-section than the ball head in a plane perpendicular to the longitudinal axis of the coupling member; and - the anchoring member comprising a threaded shaft adapted for insertion into the bone and a head portion including a cavity sized and shaped to receive the ball 15 head, the cavity surrounded by a wall of the head portion, the wall including four slots extending axially from a rim of the wall toward the threaded shaft, the slots providing the required flexibility to achieve the snap-fit connection and sized to mate with a fastener driver for driving the anchoring member into the bone; - wherein the ball head of the coupling member and the cavity in the head portion of 20 the anchoring member are structured such that, in the implanted state of the glenoidal component, the first longitudinal axis of the anchoring member diverges from the second longitudinal axis of the coupling member such that the first and second longitudinal axes are noncoaxial and nonparallel.

Accordingly, the coupling means of the prosthetic component and the separate 25 bone anchoring means are adapted to achieve a tight-fit connection or a form-fit connection, in particular a snap-fit connection, with each other.

Providing at least one separate bone anchoring means allows fixing the prosthetic component independently from the prosthetic component to the bone which in many cases facilitates the implantation procedure. The prosthetic component, 30 which is in an implanted state in direct contact with the bone via its bone contacting surface, can then be attached to said bone anchoring means. The

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connection between the prosthetic component and the separate bone anchoring means can –

as outlined above - be a tight-fit or a form-fit connection, such as a snap-fit connection. In particular, the connection is not permanent, i.e. the prosthetic component can be detached from the bone anchoring means, e.g. during revision procedures. The coupling means providing at least one of the various types of connec-

5 tions described above can be realized by simple constructive features. Moreover, tight-fit and form-fit connections in most cases do not require the use of specialized tools during implantation. The coupling means comprises and/or consist of coupling features such that coupling features provided on the prosthetic component and on the anchoring means may be interconnected with each other to connect the prosthetic component to the bone anchoring means.

10 A simple yet reliable embodiment of the set according to the present disclosure may be limited to the prosthetic component and a single bone anchoring means. In this case an articulation surface of the prosthetic assembly cooperating with other artificial or natural components of the joint is provided on the prosthetic component. Of course, the prosthetic assembly may comprise more elements in addition to the prosthetic component and a single bone anchoring means. It is e.g. conceivable to provide the articulation surface on a separate component that can be mounted to the prosthetic component. Alternatively or additionally, more than one - in particular exactly two - separate bone anchoring means may be provided.

15 20 In further embodiments, a coating promoting bone ingrowth may be provided on either one of the bone contacting surface of the prosthetic component or the bone anchoring means. Also, a porous material enabling bone ingrowth may be provided on either one of the bone contacting surface of the prosthetic component or the bone anchoring means. Said porous material may be provided as a coating, or as a material layer forming part of the structure of the prosthetic component or said at least one bone anchoring means.

25 It is also conceivable to couple the prosthetic component and the at least one bone anchoring means prior to implantation.

30 In an embodiment of the set according to the present disclosure, one of the coupling means and the bone anchoring means comprises a male coupling feature and the other one of the coupling means and the bone anchoring means compris-

es a female coupling feature adapted to receive the male coupling feature. The male coupling feature may comprise a bulge or a male taper. For instance, the male coupling feature may comprise a base portion and a head portion, the base portion having a smaller cross-section than the head portion in a plane perpendicular to a longitudinal extension of the base portion. In particular, the head portion comprises a ball head.

The coupling means may comprise a peg that is arranged on and extending from the bone contacting surface, the peg having a proximal end and a distal end, the proximal end arranged fixed to the bone contacting surface. The peg may be at-

10 attached to or be formed monolithic with the bone contacting surface of the prosthetic component. A coupling feature may be arranged on the peg. In particular each coupling feature of the prosthetic component may be provided on a peg, and/or each peg is furnished with a coupling feature. The number of pegs and the number of coupling features of the prosthetic component may in particular be the same, 15 and each coupling feature may be provided with one single coupling feature. Multiple pegs may be arranged such that their longitudinal axes extend parallel to each other. Further, all pegs may be arranged with their longitudinal axis parallel to each other.

In a further embodiment of the set according to the present disclosure, a female 20 coupling feature provided on either the prosthetic component or the bone anchoring means comprises a cavity or a female taper. A female coupling feature may be formed by a wall surrounding a cavity, said cavity being configured to receive a male coupling feature. Said cavity may be open at a rim of the wall. In one even more specific embodiment the cavity may form an undercut beyond the rim of the 25 wall thus forming a cavity which in particular serves as a female form-fit coupling feature. There may furthermore be provided at least one slot extending axially from the rim of the wall. Said slot will for instance increase the flexibility of the wall which is particularly useful to insert a male form-fit coupling feature across a bottleneck formed at the rim of the wall into the undercut area of the cavity. It will be 30 well appreciated that in certain embodiments the male coupling feature will at least over parts of its surface snugly fit into the undercut area of the female coupling feature.

In yet another embodiment of the set according to the present disclosure, two or more coupling features are provided on the prosthetic component to improve the coupling between the prosthetic component and the bone anchoring means. A number of bone anchoring means may be provided such that the number of coupling features provided by the bone anchoring means corresponds to the number of coupling features provided on the prosthetic component. A number of bone anchoring means may be provided such that the number of coupling features provided by the bone anchoring means corresponds to the number of coupling features provided on the prosthetic component. It is well understood

5 coupling features provided by the bone anchoring means corresponds to the number of coupling features provided on the prosthetic component. In one embodiment each bone anchoring means is provided with one coupling feature and consequently the number of bone anchoring means provided will be equal to the number of coupling features provided on the prosthetic component. It is well understood
10 that a coupling feature provided on the prosthetic component and a corresponding coupling feature on the bone anchoring means should be complementary in the sense that the coupling features need to be adapted to fit and lock with each other.

At least two separate bone anchoring means may be provided, wherein each of the coupling means provided on the prosthetic component is associated with one
15 of the bone anchoring means. Said embodiment may be found useful to enhance the distribution of the loads induced by the bone anchoring means. One embodiment of the set comprises exactly two bone anchoring means, each provided with one single coupling feature, and exactly two respective coupling features provided on the prosthetic component.

20 However, it is possible to choose the number of coupling features freely as needed to ensure a reliable fixation of the prosthetic component to the at least one bone anchoring means. It is even conceivable to provide both male and female coupling features on the prosthetic component and to provide the bone anchoring means with a complementary arrangement of coupling features and/or to provide two or
25 more separate bone anchoring means. For example a peg of the aforementioned kind and/or a bone anchoring means may comprise more than one coupling features.

In a further embodiment of the set according to the present disclosure, the female coupling feature is provided on a bone anchoring means.

In a further embodiment of the set according to the present disclosure, the prosthetic component is made at least partly or entirely from a synthetic material, in particular from plastic such as polyethylene.

The at least one bone anchoring means may comprise a distal bone anchoring

5 section and a proximal head section. The bone anchoring section may be formed as a threaded shank, wherein any one of the core diameter and the outer thread diameter may be cylindrical or tapering. As it will be appreciated any thread form known in orthopedic surgery will be possible, including, but not limited to, continuous, interrupted, self-tapping and double-lead threads. It will furthermore be appreciated that the bone anchoring section may be formed in any other manner suitable to provide adequate bone fixation, such as, but not limited to, press fit in the bone, cementing, or fixation through structures formed on the bone anchoring section, such as for instance a porous surface or barbs. The head section may comprise or be formed as a coupling feature. It will be well understood that a coupling feature provided on a bone anchoring means intended for being coupled with a coupling feature provided on the prosthetic component will be a counterpart coupling feature to that provided on the prosthetic component.

The bone anchoring means will in one embodiment be provided with a socket for a tool enabling inserting the bone anchoring means into the bone. In particular if the

20 bone anchoring section is formed as a thread there may be provided a socket for a screwing tool. In one exemplary embodiment the may for instance be provided a slot as to receive a screwdriver. The head may for instance be formed by a wall, said wall surrounding a cavity forming a female form fit coupling feature wherein the wall comprises an axial slot which serves to enhance the elasticity of the wall and may at the same time serve as a screwdriver socket, as exemplarily lined out above. In another exemplary embodiment there may be provided a ball head as a male coupling feature, said ball head being provided with a hex socket or a cross recess on a proximal face.

The bone anchoring means may be made from any suitable material having ap-

30 propriate mechanical properties. It will be understood that the bone anchoring means will be made from a biocompatible material, or will at least be furnished with a biocompatible cover or coating. Suitable materials may comprise, but are

not limited to, metals such as e.g. stainless steel or titanium. The bone anchoring means, and in particular the bone anchoring section, may be at least partly furnished with a coating promoting bone on-growth or a porous material allowing bone in-growth, such as for instance Zimmer Trabecular Metal™. It is further understood that such coatings or porous material will be most effective when applied to a threaded shank or any other part of the bone anchor intended to effect the anchor-bone connection. The bone anchoring means may comprise, at least in parts of its extent, a solid core surrounded by a sleeve of such porous material, or a tip made of such porous material, analogously to the lag screw disclosed in

5 10 WO2008/102016.

The present disclosure also relates to a prosthetic component for an artificial joint, in particular for a shoulder prosthesis. The prosthetic component is in particular suited to be used in embodiments of the set described herein. The prosthetic component has an articulation surface and a bone contacting surface contacting

15 the bone in an implanted state of the prosthetic component. The bone contacting surface of the prosthetic component is provided with at least one coupling means. Said coupling means may comprise a male or a female coupling feature, such as a male or a female form-fit or tight-fit coupling feature. The coupling feature may be provided on a peg, said peg being provided on and projecting from the bone contacting surface. For instance, a male form-fit coupling feature may comprise a ball

20 head provided on a distal end of a peg, the peg in turn being provided on and extending from the bone contacting surface. More than one peg and/or more than one coupling feature may be provided.

A method for implanting a set according to any of the embodiments described

25 above may comprise placing the at least one bone anchoring means in a bone of a patient and coupling the prosthetic component to the bone anchoring means. In particular, prior to the step of placing the bone anchoring means in the bone of the patient and/or the step of coupling the prosthetic component to the bone anchoring means, the bone is resected to form a component contacting surface adapted to

30 be in contact with the prosthetic component. In particular the mentioned method steps may be carried out in said order.

According to an embodiment of the method, holes for receiving an anchoring section of the bone anchoring means are formed in the bone of the patient, in particular by drilling or milling, prior to placing the bone anchoring means. The holes formed in the bone of the patient may be smaller than an outer dimension of the

5 anchoring section of the bone anchoring means and larger than or essentially equal to a core diameter of the anchoring section. The holes formed in the bone of the patient may be smaller than a core diameter of the anchoring section such as to achieve a compression of bone stock upon placing the bone anchoring means.

A countersink may be provided in the patient's bone and the bone anchoring

10 means may be placed such that the anchoring section and the head section are fully received within the bone. The method may comprise selecting areas of relatively denser and/or more stable bone stock, as compared to the overall available bone stock and selecting the location and direction of the insertion of the anchoring means to place the anchoring sections at least partly in said areas.

15 The features and embodiments described above may be readily combined with each other.

More areas of applicability of the present invention will become apparent from the detailed description provided hereinafter. It should be understood that the detailed description and specific examples are intended for the purpose of illustration only

20 and are not intended to limit the scope of the invention in any way. The drawings are simplified and schematic. Details not necessary for the understanding of the invention are omitted.

The present disclosure will be explained in more detail and become fully understood from the detailed description and the accompanying drawings.

25

Fig. 1 shows a first embodiment of a prosthetic component according to the present disclosure,

Fig. 2 shows a first embodiment of a bone anchoring means according to the present disclosure,

Fig. 3a and 3b show a set comprising the prosthetic component of Fig. 1 and two bone anchoring means according to Fig. 2 in different mounting situations,

Fig. 4 shows a top view of the bone anchoring means of Fig. 2, and

5 Fig. 5 shows second embodiments of a prosthetic component and bone anchoring means according to the present disclosure.

Fig. 1 shows a prosthetic component 10 which is used to replace a damaged natural glenoid surface of a natural shoulder joint. An articular surface 12 of prosthetic 10 component 10 mimics the geometry of the natural glenoid surface. Alternatively, the geometry of said surface may be optimized for cooperation with further prosthetic components of the artificial joint, such as a prosthetic humeral articular surface or an articular surface of a bearing component disposed between prosthetic component 10 and a humeral component of the shoulder prosthesis. The shape of 15 articular surface 12 may be symmetrical or asymmetrical.

Prosthetic component 10 is in an implanted state in direct contact with the surrounding bone. Specifically, a bone contacting surface 14 directly contacts the scapula of the patient in an implanted state. Hence, there is no intermediate component provided which is disposed between the bone surface and prosthetic component 10. The bone surface may be resected to make sure that bone contacting 20 surface 14 of prosthetic component 10 snuggly fits on the bone surface.

It is conceivable to provide a multipartite prosthetic component, e.g. wherein the articular surface and the bone contacting surface are provided on separate but (releasably) joinable elements. Thus, these joinable elements form in a mounted 25 state a multi-part assembly. Mounting of said elements may take place prior to the connection of the element carrying the bone contacting surface to the bone anchoring means or later.

Two pegs 16 extend from bone contacting surface 14. Pegs 16 comprise an essentially cylindrical base portion 18 carrying an essentially spherical ball head 20,

said spherical ball head providing a male form fit coupling feature. However, deviations of a spherical shape are conceivable.

Prosthetic component 10 is - as can be seen from Fig. 1 - provided with two pegs 16 disposed symmetrically with respect to a midplane P1, which in the shown

5 embodiment also represents a symmetry plane of surfaces 12, 14. However, it is also possible to provide an asymmetrical design of surfaces 12, 14 and/or an asymmetrical arrangement of pegs 16 on bone contacting surface 14 with respect to midplane P1.

Both pegs 16 extend from bone contacting surface 14 in a direction parallel to

10 plane P1. In other words, each peg 16 defines a longitudinal axis A1, A2, respectively, which is arranged parallel to plane P1. A respective center C of ball heads 20 lies on longitudinal axes A1, A2, respectively.

For specific applications, it might be envisaged to provide pegs 16 having longitudinal axes A1, A2 that are not disposed symmetrically with respect to plane P1

15 and/or which are not parallel to plane P1. The longitudinal extension of pegs 16 and the geometry of the respective ball heads 20 may be chosen in accordance with the constraints of the specific case and/or the joint geometry or kinematics. It is also not imperative to provide pegs with identical or similar design. To ensure proper installation - especially in case a prosthetic component 10 of asymmetrical 20 design is used - it might be helpful to provide pegs having distinctly different design. These pegs then may be coupled only to bone anchoring means of complementary design so that there is only one way - namely the correct way - of mounting the corresponding prosthetic component to the bone.

E.g. in deviation from the design shown in Fig. 1, prosthetic component 10 may

25 have a first peg 16 that is provided with a female coupling feature and a second peg 16 as depicted in Fig. 1. Further, instead of two pegs 16 only one peg 16 or more than two pegs 16 may be provided.

Fig. 2 shows a bone anchoring means 22 comprising a threaded shank 24 and a head portion 26. Head portion, or distal end, 26 is provided with a cavity 28 (indicated by dashed lines) designed to receive ball head 20 of pegs 16, thus providing

30 a female form-fit coupling feature. Head portion 26 further comprises slots 30

extending parallel to longitudinal axis A3 of bone anchoring means 22. Head portion 26 is designed such that a ball head 20 as illustrated in Fig. 1 can be snapped into said head portion 26.

Exemplarily, two bone anchoring means 22 are mounted in an appropriate way

5 into the resected scapula of a patient. Slots 30 facilitate the use of a suitable screwdriver to screw means 22 in the bone. Then, prosthetic component 10 is snapped onto bone anchoring means 22 through impacting the articular surface 12 in a direction approximately parallel to axes A1, A2 of pegs 16.

Fig. 3a and 3b each show an example of a set comprising prosthetic component

10 10 and two bone anchoring means 22 in a mounted state (bone omitted for clarity). In the example shown in Fig. 3a, longitudinal axes A3 of bone anchoring means 22 diverge when seen from bone contacting surface 14. In Fig. 3b, a convergent arrangement of axes A3 is shown.

While in the exemplary embodiments shown in Fig. 3a, 3b the bone anchoring

15 means 22 are arranged with some symmetry with respect to the prosthetic component 10, it will be appreciated that the bone anchoring means 22 need not necessarily to be arranged with any symmetry nor need they be arranged in a common plane. Due to the ball-and-socket joint type connection between the coupling features 20, 28 provided on the prosthetic component 10 and those provided on
20 the bone anchoring means 22, respectively, the bone anchoring means 22 may be arranged in a variety of spatial orientations with respect to prosthetic component 10. In other words, the orientation of the bone anchoring means 22 as implanted into the patient can be chosen relatively freely. The prosthetic component 10 only imparts few geometrical constraints as regards the position and orientation of the
25 implanted bone anchoring means 22. This allows the surgeon to implant the bone anchoring means 22 in regions of the bone where good bone quality can be expected.

It will also be appreciated that male and female coupling features provided on the

30 prosthetic component 10 and a bone anchoring means 22 may be swapped. It will further be appreciated that female as well as male coupling features may be provided on the prosthetic component 10 and the corresponding bone anchoring

means 22 then will be chosen to have a complementary coupling feature. The orientation of bone anchors 22 in the bone of the patient may be chosen as required to achieve a reliable fixation. The orientation of bone anchoring means 22 may take the bone quality and other aspects, such as implantation procedures, 5 into account to achieve optimum results. Contrary to conventional concepts, the coupling concept to mount prosthetic component 10 to bone anchoring means 22 comprising in the depicted embodiment a snap-fit connection between ball heads 20 on pegs 16 engaging cavities 28 in head portions 26 of anchors 22 allows a multitude of different bone anchoring means placement geometries, thus giving 10 greater flexibility with one and the same prosthetic component.

Fig. 4 shows a top view of head portion 26 of bone anchoring means 22 revealing that slots 30 not only provide the required flexibility of walls 32 defining cavity 28 necessary to realize a snap-on connection but they can also be used to screw bone anchoring means 22 into the bone of the patient. In other words, slots 30 can 15 be engaged by an appropriate tool, such as a screwdriver, to screw bone anchoring means 22 into the bone.

Fig. 5 shows a configuration of a set for connecting a prosthetic assembly of an artificial wherein the prosthetic component 10' of said assembly is provided with a female coupling feature 28' and a single bone anchoring means 22' is provided 20 with the complementary male coupling feature 20'. In other words, proximal end portion 16' of the bone anchoring means 22' comprises ball head 20' providing a male coupling feature and adapted to be received in the female coupling feature 28' provided on the prosthetic component 10'. Female prosthetic component coupling feature 28' - in the embodiment shown in Fig. 5 a cavity - may likewise be 25 provided on a peg 16, analogous to male coupling feature 20 shown in Fig. 1.

It should be understood, that the ball-snap mechanism shown in two alternative variants in Figs. 1 to 5 may be replaced or complemented by other types of connection such as a press-fit connection, e.g. a taper lock connection, and/or other types of a form-fit connection. I.e. embodiments of the set according to the present 30 disclosure are conceivable that are provided with two or more different types of connections. Multiple types of connectors may be provided at different locations of a prosthetic component.

The connection(s) between a prosthetic component 10, 10' and bone anchoring means 22, 22' may be releasable to allow an easy replacement of the prosthetic component 10, 10'. Bone cement may be additionally used, if necessary. In special cases, prosthetic component 10, 10' may also be cemented directly to the bone.

- 5 The description is mainly of exemplary nature and, thus, any modifications and variants that do not depart from the gist of the disclosed teachings are intended to be within the scope of the disclosure.

Reference numeral list

10	10, 10'	prosthetic component
	12	articular surface
	14, 14'	bone contacting surface
	16	peg
	16'	proximal end portion
15	18	base portion
	20, 20'	ball head
	22, 22'	bone anchoring means
	24	threaded shank
	26	head portion
20	28, 28'	cavity
	30	slot
	32	wall
	34	mounting portion
	P1	mid plane
25	A1, A2, A3	longitudinal axis
	C	center

The claims defining the invention are as follows:

1. A set for connecting a prosthetic assembly of an artificial shoulder joint to a bone, the set comprising:
 - a glenoidal component comprising a bone contacting surface adapted for contacting the bone in an implanted state of the glenoidal component and an opposed articular surface adapted for contacting an articular surface of a humeral component or a bearing component; and
 - a separate bone anchoring member extending along a first longitudinal axis, wherein the bone contacting surface of the glenoidal component is provided with a coupling member extending along a second longitudinal axis and adapted to be coupled to the bone anchoring member in the implanted state of the glenoidal component, and wherein the coupling member and the bone anchoring member are adapted to achieve a tight-fit connection with each other;
 - the coupling member comprising a peg extending from the bone contacting surface of the glenoidal component and an essentially spherical ball head disposed at an end of the peg, the peg having a smaller cross-section than the ball head in a plane perpendicular to the second longitudinal axis of the coupling member; and
 - the anchoring member comprising a threaded shaft adapted for insertion into the bone and a head portion including a partially spherical cavity sized and shaped to receive the ball head, the head portion defining a cavity opening at a distal end of the anchoring member, the cavity shaped to define a portion of a sphere truncated at the cavity opening, wherein a height of the cavity defined between the cavity opening and an opposing bottom surface of the cavity is less than a diameter of the ball head such that a portion of the ball head remains exposed when the coupling member and the anchoring member are attached;

- wherein the ball head of the coupling member and the cavity in the head portion of the anchoring member are structured such that, in the implanted state of the glenoidal component, the first longitudinal axis of the anchoring member diverges from the second longitudinal axis of the coupling member such

5 that the first and second longitudinal axes are noncoaxial and nonparallel.

2. A set for connecting a prosthetic assembly of an artificial shoulder joint to a bone, the set comprising:

- a glenoidal component comprising a bone contacting surface adapted for contacting the bone in an implanted state of the glenoidal component and an opposed articular surface adapted for contacting an articular surface of a humeral component or a bearing component; and
- a separate bone anchoring member extending along a first longitudinal axis,

10 wherein the bone contacting surface of the glenoidal component is provided with a coupling member extending along a second longitudinal axis and adapted to be coupled to the bone anchoring member in the implanted state of the glenoidal component, and

15 wherein the coupling member and the bone anchoring member are adapted to achieve a snap-fit connection with each other;

- the coupling member comprising a peg extending from the bone contacting surface of the glenoidal component and a ball head disposed at an end of the peg, the peg having a smaller cross-section than the ball head in a plane perpendicular to the longitudinal axis of the coupling member; and
- the anchoring member comprising a threaded shaft adapted for insertion into the bone and a head portion including a cavity sized and shaped to receive the ball head, the cavity surrounded by a wall of the head portion, the wall including four slots extending axially from a rim of the wall toward the threaded shaft, the slots providing the required flexibility to achieve the snap-fit connection and sized to

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mate with a fastener driver for driving the anchoring member into the bone;

- wherein the ball head of the coupling member and the cavity in the head portion of the anchoring member are structured such that, in the implanted state of the glenoidal component, the first longitudinal axis of the anchoring member diverges from the second longitudinal axis of the coupling member such that the first and second longitudinal axes are noncoaxial and nonparallel.

10 3. The set according to claim 1 or 2, wherein at least two coupling members are provided on the glenoidal component.

15 4. The set according to claim 3, wherein at least two separate bone anchoring members are provided and wherein each of the coupling members provided on the glenoidal component is associated with one of the bone anchoring members.

20 5. The set according to claims 3 or 4, wherein the at least two coupling members are arranged in parallel.

6. The set according to any of claims 1 to 5, wherein the cavity is surrounded by a wall of the head portion, and wherein said wall is provided with at least one slot extending axially from a rim of the wall toward the threaded shaft.

25 7. The set according to any of claims 1 to 6, wherein the glenoidal component is made at least partly from a synthetic material.

8. The set according to any of claims 1 to 7, wherein bone anchoring member comprises a bone screw.

30 9. The set according to claim 4, wherein exactly two bone anchoring members and exactly two coupling members are provided.

10. The set according to any one of claims 1 to 9, wherein the bone anchoring member includes a porous layer structured to promote bone ingrowth.
- 5 11. The set according to claim 10, wherein the porous layer comprises a porous coating.
- 10 12. The set according to any one of claims 1 to 11, wherein the bone contacting surface of the glenoidal component includes a porous layer structured to promote bone ingrowth.
13. The set according to claim 12, wherein the porous layer comprises a porous coating.
- 15 14. The set according to any one of claims 1 to 13, wherein the articular surface of the glenoidal component mimics a geometry of a natural glenoid surface.
15. The set according to any one of claims 1 to 14, wherein the articular surface is symmetrical.
- 20 16. The set according to any one of claims 1 to 14, wherein the articular surface is asymmetrical.
- 25 17. The set according to claim 6, wherein said wall is provided with a plurality of slots extending axially from the rim of the wall toward the threaded shaft.

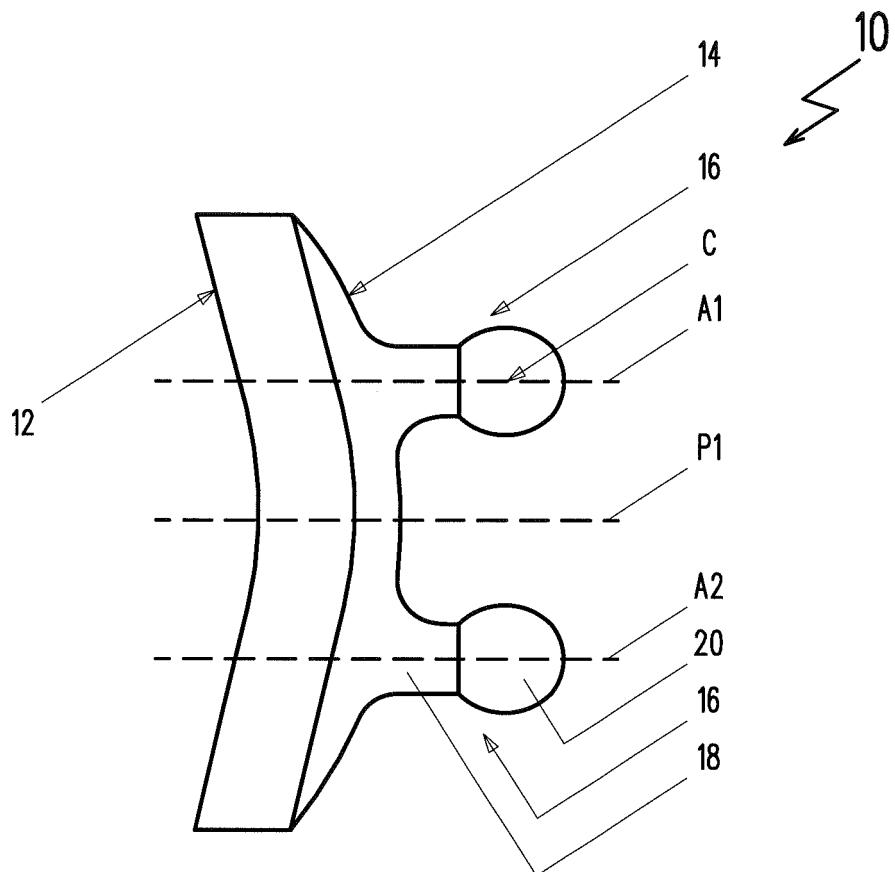


Fig. 1

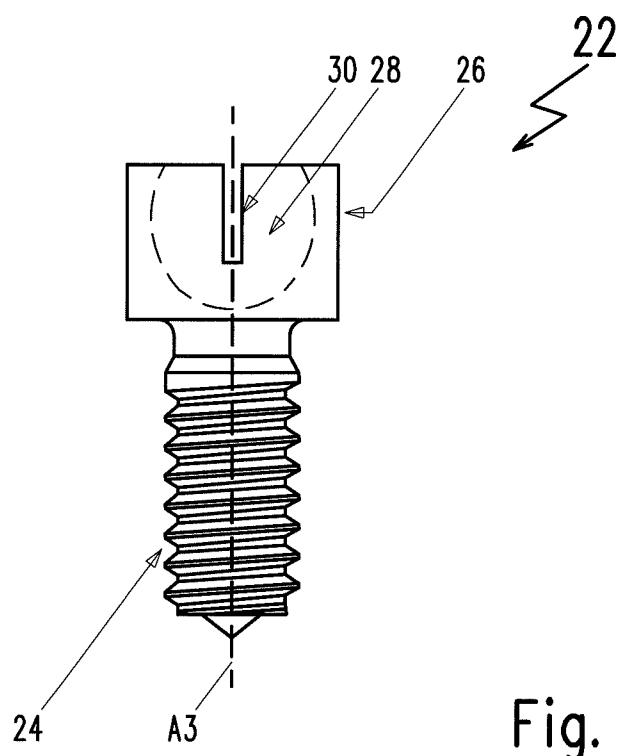


Fig. 2

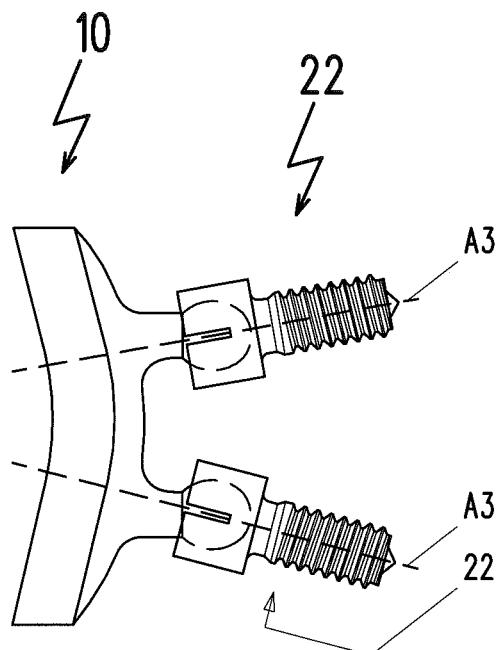


Fig. 3a

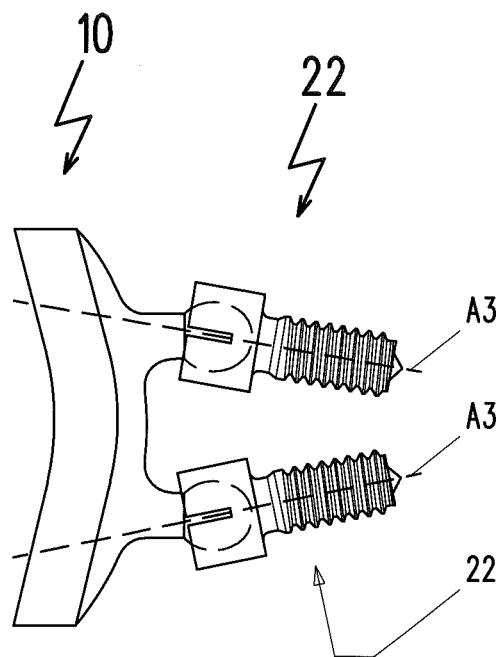


Fig. 3b

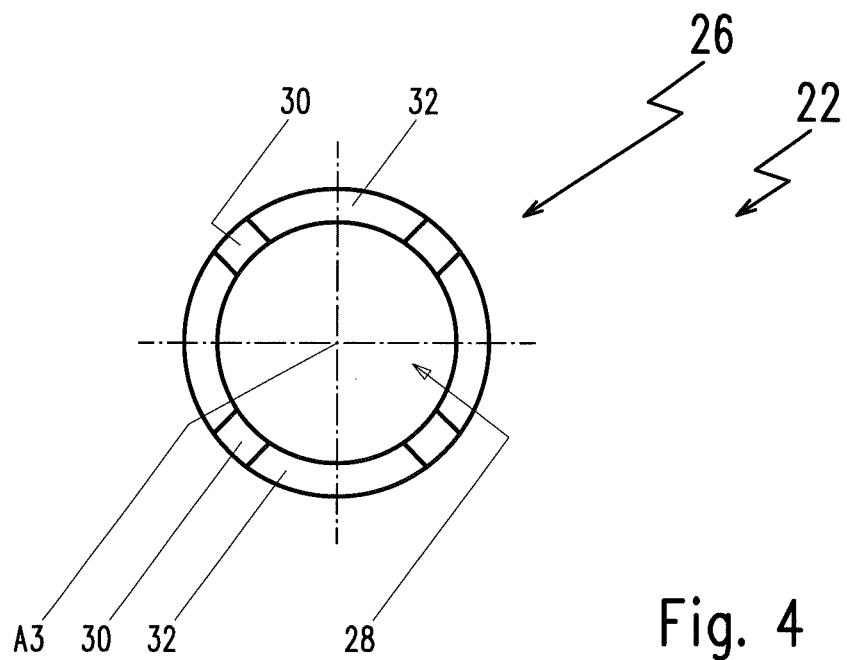


Fig. 4

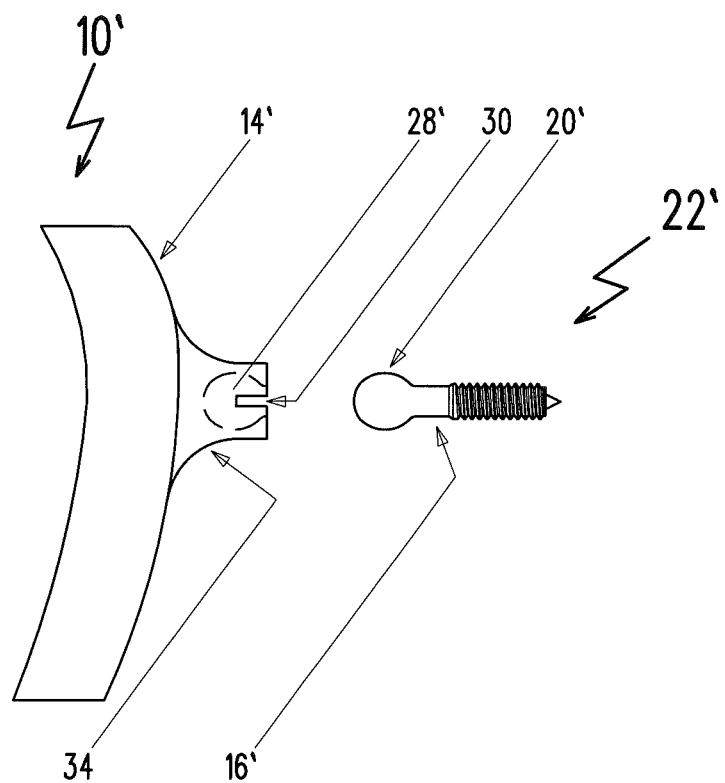


Fig. 5