

**(12) STANDARD PATENT  
(19) AUSTRALIAN PATENT OFFICE**

**(11) Application No. AU 2018227019 B2**

(54) Title  
**Surgical implant system**

(51) International Patent Classification(s)  
**A61N 1/36** (2006.01)      **A61N 1/05** (2006.01)

(21) Application No: **2018227019**      (22) Date of Filing: **2018.02.28**

(87) WIPO No: **WO18/158305**

(30) Priority Data

(31) Number  
**62/464,917**      (32) Date  
**2017.02.28**      (33) Country  
**US**

(43) Publication Date: **2018.09.07**  
(44) Accepted Journal Date: **2023.07.20**

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(56) Related Art  
**US 2014/0371802 A1**  
**US 2014/0358197 A1**  
**US 2014/0358026 A1**  
**US 2011/0071594 A1**

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property  
Organization  
International Bureau(43) International Publication Date  
07 September 2018 (07.09.2018)(10) International Publication Number  
WO 2018/158305 A1

## (51) International Patent Classification:

A61N 1/36 (2006.01) A61N 1/05 (2006.01)

## (21) International Application Number:

PCT/EP2018/054913

## (22) International Filing Date:

28 February 2018 (28.02.2018)

## (25) Filing Language:

English

## (26) Publication Language:

English

## (30) Priority Data:

62/464,917 28 February 2017 (28.02.2017) US

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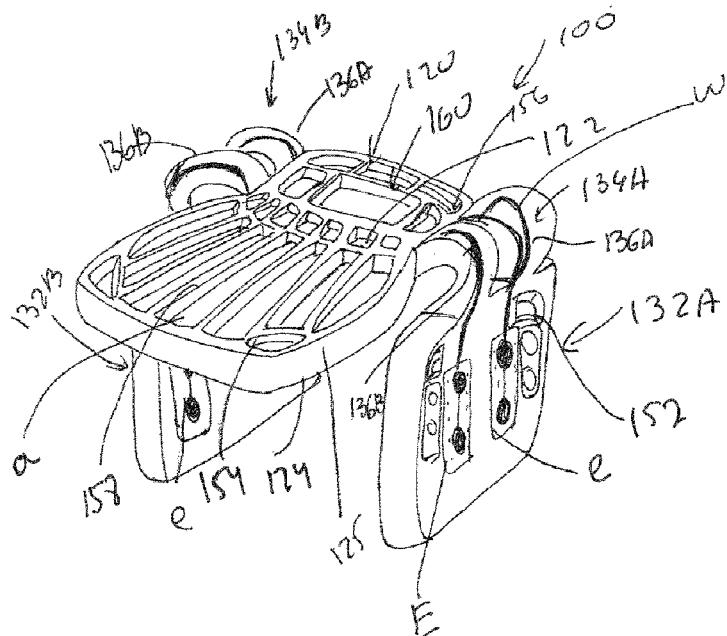
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(81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY, BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DJ, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IR, IS, JO, JP, KE, KG, KH, KN, KP, KR, KW, KZ, LA, LC, LK, LR, LS, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SA,

## (54) Title: SURGICAL IMPLANT SYSTEM





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SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ, TM, TN,  
TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

**(84) Designated States** (*unless otherwise indicated, for every kind of regional protection available*): ARIPO (BW, GH, GM, KE, LR, LS, MW, MZ, NA, RW, SD, SL, ST, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, RU, TJ, TM), European (AL, AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV, MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK, SM, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, KM, ML, MR, NE, SN, TD, TG).

**Published:**

— with international search report (Art. 21(3))

22 Jun 2023

2018227019

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## Surgical Implant System

### TECHNOLOGICAL FIELD

The disclosed subject matter is directed to a surgical implant system, device and methods related to medical conditions such as the obstructive sleep apnea. In particular, the disclosed subject matter is directed to an implant for neurostimulation and associated activation devices and methods.

### BACKGROUND

Various types of neurostimulators are known in the art. In the field of neurostimulators for the stimulation of the hypoglossal nerves, the following provide some examples, details of which are incorporated herein by reference.

US 8,577,465 describes an implant unit that may include a flexible carrier, at least one pair of modulation electrodes on the flexible carrier, and at least one implantable circuit in electrical communication with the at least one pair of modulation electrodes. The at least one pair of modulation electrodes and the at least one circuit may be configured for implantation through derma on an underside of a subject's chin and for location proximate to terminal fibers of the medial branch of the subject's hypoglossal nerve, such that an electric field extending from the at least one pair of modulation electrodes can modulate one or more of the terminal fibers of the medial branch of the hypoglossal nerve.

US2013085560 describes an implant unit configured for implantation into a body of a subject and may include an antenna configured to receive a signal. The implant unit may also include at least one pair of modulation electrodes configured to be implanted into the body of the subject in the vicinity of at least one nerve to be modulated, the at least one pair of modulation electrodes being configured to receive an applied electric signal in response to the signal received by the antenna and generate an electrical field to modulate the at least one nerve from a position where the at least one pair of modulation electrodes does not contact the at least one nerve.

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The following provides for an example of an activation tool used to active a neurostimulator during the surgical procedure. US201403189 disclosure of which is incorporated herein by reference, describes an implant unit delivery tool having an implant tool and an implant activator. The implant tool may be configured to retain an implant unit during an implantation procedure in which the implant unit is fixated to tissue. The implant activator may be associated with the implant tool. Additionally, the implant activator may be configured to selectively transfer power to the implant unit during the implantation procedure to cause modulation of at least one nerve in the body of a subject prior to final fixation of the implant unit to the tissue.

Any discussion of documents, acts, materials, devices, articles or the like which has been included in the present specification is not to be taken as an admission that any or all of these matters form part of the prior art base or were common general knowledge in the field relevant to the present disclosure as it existed before the priority date of each of the appended claims.

## GENERAL DESCRIPTION

Throughout this specification the word "comprise", or variations such as "comprises" or "comprising", will be understood to imply the inclusion of a stated element, integer or step, or group of elements, integers or steps, but not the exclusion of any other element, integer or step, or group of elements, integers or steps. The term "includes" means includes but not limited to, the term "including" means including but not limited to.

In one aspect of the disclosed subject matter, there is disclosed a surgical implant. The surgical implant in accordance with this aspect comprises:

- a) a substantially planar central body portion having a top side and a bottom side;
- b) at least two adjustable wing portions, each of the at least two adjustable wing portions including one or more electrodes for emitting an electrical field;
- c) at least two connecting members, each one of the at least two connecting members extending from opposite sides of the central body portion, the each one of the at least two connecting members being configured for flexibly connecting each one of the at least two wing portions at opposite sides to said central body portion, wherein the central body portion is further provided with an internally disposed load bearing reinforcing structure, configured to provide structural rigidity to the central body portion, and wherein the wing portions are more flexible than the central body portion.

Any one of the following embodiments may apply to any one of the aspects of the disclosed subject matter, alone or in combination:

- the central body may have one side substantially planar and an opposite side having at least a partially arched surface.
- the wings and the central body portion may be made from the same material.
- the wings and the central body portion may be made from different materials.
- the flexible connection is via a hinge and the hinge portion is thinner than an adjacent portion of the wing of which it is a part.
- each one of said at least two connecting members extend from the central body through at least one hinge member.
- each one of said at least two connecting members extend from the central body through at least one hinge member and wherein each one of said at least two wing portions being hingedly articulated to the at least one hinge through an extension member extending between the central body portion and the at least one of the at least two wing portions.
- the connecting member may be a flexible element configured to deform in at least one direction.
- the flexible element may be in the form of a flexible arch permitting bending movement along its length in a first direction such that the central body and each of the at least two wing portions flex away from each other.
- Further may comprise a flexible arch comprising:
  - 25 at least one central segment arranged along the length of the flexible arch; and at least two hinge structures, each one of the hinge structures being disposed between the central body and the at least one central segment and the one of
  - 30 the at least two wing portions and the central segment and oriented in a direction transverse to the length of the central segment.
- the flexible arch may be formed from a unitary elastomeric material and the hinges comprise living hinges.
- the flexible arch may be formed from multiple segments; the multiple segments may be connected through living hinges; the multiple segments may be connected through material, the material may have a thickness less

than the thickness of the segments.

- the flexible arch may have a narrowing width, having the largest width at the area of connection to the central body and a narrower width at the area of connection with at least one of the wing portions.
- the flexible arch may have a non-uniform thickness and/or a non-uniform width.
- the surgical implant may be formed from a unitary elastomeric material.
- the surgical implant may comprise at least one anchoring arrangement.
- the surgical implant may comprise at least one anchoring arrangement, wherein the anchoring arrangement may be in a form of at least one suture hole.
- the surgical implant may comprise at least one anchoring arrangement, wherein the anchoring arrangement may be in a form of at least one suture hole, wherein the at least one suture hole is provided on the central body portion and/or the at least one of the at least two wing portions.
- the anchoring arrangement may be in the form of a suture hole, the suture hole may be reinforced internally and/or externally.
- the reinforced anchoring arrangement may comprise an embedded reinforcing element.
- the reinforced anchoring arrangement may comprise an embedded reinforcing element and/or a reinforcing layer of material forming part of the arrangement.
- the reinforcing anchoring arrangement may be a mesh material.
- the anchoring arrangement may be part of the load bearing reinforcing element of the implant;
- the surgical implant may comprise at least one anchoring arrangement, wherein the anchoring arrangement may be configured for anchoring the surgical implant at the implant location, anchoring at least said at least two wing portions opposite one from the other.
- the anchoring arrangement is configured to prevent damage to at least a portion of the internal components of the surgical implant.
- the implant unit may comprise an anchoring arrangement which may be

chemical or mechanical; in some embodiments, the anchoring arrangement may comprise an adhesive. In another embodiment, the anchoring arrangement may comprise staples, sutures, absorbable sutures, a mechanical encapsulation of at least a portion of the implant unit within the body.

- the at least two wing portions may have at least one degree of freedom and may be flexibly adjustable to various angular dispositions with respect to the main body.
- the at least two wing portions may have at least one degree of freedom and may be flexibly adjustable to various angular dispositions with respect to the main body, and wherein the angular disposition may be between 0 to up to 270 degrees; in accordance with an embodiment, the angular disposition may be between -90 to up to 270 degrees.
- the at least two wing portions may have at least one degree of freedom and may be flexibly adjustable to various angular dispositions along more than one axis and in some embodiments, along and/or around three axis.
- the at least two wing portions have more than three degrees of freedom and may be flexibly adjustable to various angular dispositions with respect to the main body and/or the connecting members.

the flexible arch is formed from a unitary elastomeric material and the hinges comprise living hinges.

- at least in one configuration of the implant device, the flexible arch may protrude beyond the top side of the substantially planar surface of the central body.
- at least in one configuration of the implant device, the flexible arch may protrude at an angle beyond the planar surface of the top side of the central body.
- at least the central body portion is further provided with internally disposed load bearing reinforcing structure, configured to provide structural rigidity to the central body portion; in one embodiment the reinforcing structure may be a system of elements; in another embodiment the reinforcing structure may be a unitary element.
- the load bearing reinforcement structure may be formed from any

suitable material configured to hold structural integrity under exertion of force thereupon.

- The load bearing reinforcement structure may be formed from any one of a polymer, polyether ether ketone (PEEK), ULTEM, liquid crystal polymer (LCP), ceramics, or alloy of compatible materials or combination of materials.
- the implant may be substantially encapsulated at least in one layer of a biocompatible polymer including at least one of silicone, phenyltrimethoxysilane (PTMS), polymethyl methacrylate (PMMA), parylene C, polyimide, liquid polyimide, laminated polyimide, epoxy, polyether ether ketone (PEEK), liquid crystal polymer (LCP), KAPTON, or combinations thereof.
- the implant may be encapsulated at least in one layer of a biocompatible polymer, and include one or more additional layer covering portions thereof.
- the implant may be encapsulated at least in one layer of a biocompatible material, and may include ceramic material, thermoplastic material such as ULTEM, or other compatible materials.
- the central body portion may be provided with an antenna configured to receive a signal and wherein each one of the at least two wing portions is provided with at least a pair of electrodes in electric communication with the antenna, the electrodes being configured to receive an electric current in response to the signal received by the antenna, such that at least one of pair of electrodes is configured to emit an electrical field.
- the first pair of electrodes and the second pair of electrodes can be activated to simultaneously generate respective electric fields.  
the first pair of electrodes and the second pair of electrodes may be partially covered at their periphery with the encapsulating material, having at least a portion thereof exposed.
- the first pair of electrodes and the second pair of electrodes may be partially embedded within the encapsulating material and comprise an outer layer of encapsulating material extending thereover and leaving at least a portion thereof exposed to the environment.

- the surgical implant is configured to conform to an exterior surface of a genioglossus muscle of a subject, such that the at least two wing portions are positioned at the sides of the genioglossus muscle adjacent to terminal fibers of a medial branch of a hypoglossal nerve, and wherein the electrodes generate electric field sufficient to modulate the terminal fibers of a medial branch, when spaced apart thereof.
- at least one of the first pair of electrodes and the second pair of electrodes are connected to electric circuitry through wires.
- at least one of the first pair of electrodes and the second pair of electrodes are connected to electric circuitry through wires, the circuitry being disposed on the central body and the wires being configured to extend through the respective connecting members.
- the wires may be disposed such that the integrity of the communication between the electric circuitry and the electrodes is not impaired when at least one of the connecting members is displaced.
- the wires may be coiled wires.
- the wires may be undulating.

In another aspect of the disclosed subject matter there is disclosed an implant unit activation device, comprising: a main body comprising an implant activator and an axially displaceable adaptor configured to displace relative the main body, the implant activator having a power source and being configured to wirelessly transfer energy from the power source to an implant unit during implantation of the implant unit into the body of a subject to cause stimulation of at least one nerve in the body of the subject; and wherein the axial displacement of the adaptor allows adjusting of the amount of energy received by the implant unit.

The amount of energy may be adjusted directly through the implant unit activation device.

In yet another aspect, there is provided a method of positioning and activating a surgical implant according to any one of the above aspects, wherein the surgical implant is a neurostimulation implant device, the method comprising:

providing a surgical implant according to any one of the above aspects, device having:

a central body portion provided with a first antenna configured to receive a signal;

at least a first pair of electrodes and a second pair of electrodes

operatively coupled to a central body portion;

wherein the central body portion is in electric communication with at least the first pair of electrodes and the second pair of electrodes, said at least first pair of electrodes and the second pair of electrodes being configured to receive an electric signal in response to the signal received by the first antenna, such that at least one of pair of electrodes is configured to emit an electrical field to stimulate a nerve in a subject's body,

providing an implant unit activation device, the implant unit activation device comprising: a main body comprising an implant activator having a power source, a second antenna configured to provide a signal to the first antenna and an axially displaceable adaptor/retractor associated with the implant activator, the implant activator configured to wirelessly transfer energy from a power source comprised therein to the neurostimulation device during implantation to cause stimulation of at least one nerve in the body of the subject; and

wherein the axial displacement of the adaptor\retractor from at least a first position to at least a second position allows adjusting of the degree of energy received by the implant unit;

identifying the stimulation threshold by determining a degree of nerve stimulation response for each of the at least first pair of electrodes and a second pair of electrodes by positioning said first pair of electrodes at an estimated implant location proximal to the nerve and selectively displacing the second antenna by repositioning the main body with respect to the adaptor/retractor to deliver a first amount of current and a second amount of current required to obtain a stimulation threshold in at least the first pair of electrodes based on one or more patient signals;

positioning the at least the second pair of electrodes at an estimated location and delivering the second amount of power required and determining a degree of nerve stimulation by the at least said second pair of electrodes.

In one embodiment the implant may be configured for treatment of obstructive sleep apnea and the location of implantation may be in the vicinity of the hypoglossal nerve. In accordance with this embodiment the neurostimulation device may be configured to modulate at least one branch of the hypoglossal nerves.

The second amount may be greater or equal to the first amount of power.

The second amount may be equal to or less relative the first amount of power.

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## BRIEF DESCRIPTION OF THE DRAWINGS

In order to better understand the subject matter that is disclosed herein and to exemplify how it may be carried out in practice, embodiments will now be described, by way of non-limiting examples only, with reference to the accompanying drawings, in which:

Fig. 1A is a perspective view of the surgical implant in accordance with one example of the disclosed subject matter;

Fig. 1B is a side view of the surgical implant of Fig. 1A;

Fig. 1C is a front view of the surgical implant of Fig. 1C;

Fig. 1D and 1E are a top and bottom plan view of the surgical implant of Fig. 1A, showing the outer contour lines thereof;

Fig. 2 is another perspective view of the surgical implant in accordance with an example of the disclosed subject matter, showing substantially transparent outer surface;

Fig. 3 illustrates the surgical implant in accordance with the disclosed subject matter, e.g. of Fig. 1, positioned over the genioglossus muscle;

Fig. 4 is a perspective side view of the implant unit activation device in accordance with one example of the disclosed subject matter;

Fig. 5 is a perspective side view of the axially displaceable adaptor of Fig. 4;

Fig. 6 is a top view of the main body of the implant activator of Fig. 4;

Fig. 7A and Fig. 7B (partially) illustrate the implant activation device of Fig 4, with the adaptor in a semi-transparent view;

Fig. 7C illustrates the implant unit activation device in a cross section along line A-A in Fig. 4.

**DETAILED DESCRIPTION OF EMBODIMENTS**

Examples of the presently disclosed subject matter relate generally to a surgical implant configured for modulating a nerve through the delivery of energy. Nerve modulation, or neural modulation, includes inhibition (e.g. blockage), stimulation, modification, regulation, or therapeutic alteration of activity, electrical or chemical, in the central, peripheral, or autonomic nervous system. Nerve modulation may take the form of nerve stimulation, which may include providing energy to the nerve to create a voltage change sufficient for the nerve to activate, or propagate an electrical signal of its own. As referred to herein, modulation of a nerve may include modulation of an entire nerve and/or modulation of a portion of a nerve. In patients with obstructive sleep apnea (OSA), for example, a primary target response of nerve stimulation may include contraction of a tongue muscle in order to move the tongue to a position that does not block the patient's airway, the cause of obstruction in OSA. While the examples of the disclosed subject matter will be discussed in relation to OSA, it will be appreciated that the features of the disclosed subject matter can be applied to surgical implant for nerve modulation for other conditions in mammalian bodies, *mutatis mutandis*. It will be further appreciated, that the presently disclosed subject matter is directed to the surgical implant, and the implant can be activated by an activator unit provided with a power source either applied externally or implanted in the body of the subject. In one example, the external activation unit for the implant is disclosed in other applications and patents to the applicant, disclosures of which are incorporated herein by reference.

Figures 1A to 1E and Figure 2 illustrate an example of the surgical implant in accordance with the disclosed subject matter. The implant may be formed of any materials suitable for implantation into the body of a patient. The implant in accordance with the disclosed subject matter is at least partially encapsulated in a biocompatible material. The implant may be substantially encapsulated at least in one layer of a biocompatible polymer including at least one of silicone, phenyltrimethoxysilane (PTMS), polymethyl methacrylate (PMMA), parylene C, polyimide, liquid polyimide, laminated polyimide, epoxy, polyether ether ketone (PEEK), liquid crystal polymer (LCP), KAPTON, or combinations thereof. In addition, the implant may be encapsulated at least in one layer of a biocompatible polymer, and include one or more additional layer covering portions thereof. It will be appreciated that the implant may include ceramic material, thermoplastic material such as ULTEM, or other compatible materials.

The surgical implant, generally designated 100, comprises a substantially planar central body portion 120 having a top side 122 and a bottom side 124; two adjustable wing portions 132A and 132B; connecting members 134A and 134B (in the illustrated example, each connecting member comprising two elements 136A and 136B as will be further described hereinafter). The connecting members extending respectively from opposite sides of the central body portion 120, each of the connecting members is configured for flexibly connecting each one of the two wing portions 132A and 132B to said central body portion 120 at opposite sides thereof.

While the description provides for the structural features of the disclosed surgical implant, in accordance with the disclosed subject matter the implant further comprises electronic components configured to stimulate a nerve when implanted in a subject in a location that permits it to modulate a nerve (e.g. as seen in Fig. 3) as will be discussed, without being in a direct contact with the nerve to be modulated/stimulated. When used to stimulate a nerve for the treatment of obstructive sleep apnea, the implant unit 100 may be placed on a genioglossus muscle so as to neuromodulate a hypoglossal nerve, which at least partially may extend within the muscle. In one example, due to the structure of the surgical implant, its flexibility and the degrees of freedom of the connecting members and the wing portions, it allows for neuromodulation of nerve branches otherwise not accessible as these are either extending within the muscle tissue or are branched out such that only emitting of electrical field over an area covering the respective branches of the nerve will permit neuromodulating of the nerve, such as the terminal branches of the hypoglossal nerve.

For example, implant may include an antenna **a** (seen e.g. in Figs 1A and 2) and associated electronic circuit and components mounted onto or integrated with central body portion (160, details not shown). The antenna **a** may include any suitable antenna known to those skilled in the art that may be configured to send and/or receive signals and power. The antenna may include any suitable size, shape, and/or configuration accommodated by the dimensions of the implant. The size, shape and/or configuration may be determined by the patient anatomy, the placement location of the implant unit, the amount of energy required to neuromodulate the nerve, etc. Suitable antennas may include, but are not limited to, a long-wire antenna, a patch antenna, a helical antenna, PCB antenna, etc.

Implant may additionally include a plurality of field-generating implant electrodes generally designated e (e.g. Fig. 1 A, 18, 2). The electrodes e may include any suitable shape and/or orientation on the implant unit so long as the electrodes may be configured to generate an electric field in the body of a patient. Implant electrodes may also include any suitable conductive material (e.g., copper, silver, gold, platinum, iridium, platinum-iridium, platinum-gold, conductive polymers, etc.) or combinations of conductive (and/or noble metals) materials. In some embodiments, for example, the electrodes may include short line electrodes, circular electrodes, and/or circular pairs of electrodes. As shown in Figure 1 B, electrodes e may be located on the wing portions connected by connecting wires W to the electronic components and the antenna on the central body portion.

The electrodes e, however, may be located on any portion of wing portions. The connecting wires are configured to extend through the connecting members and are sized and shaped to be encapsulated therein. In accordance with an example, the wires W extend in designated channels. In accordance with yet an example, the wires may extend in designated reinforced channels. In accordance with some examples, the connecting members are provided with designated channels (not shown) configured to retain the connecting wires in place and further facilitating the flexibility of the connecting members without braking or damaging the wires and their respective connections to the components on the central body portion and the respective electrode. The implant may further include circuit components 160 and any other required components facilitating the antenna to receive the energy and transmitting this energy for the electrodes to emit the electric field to the nerves. In the illustrated example, the implant does not comprise a power source. The implant in the illustrated example is activated externally. It will be appreciated that other means of activating the implant can be envisioned, either externally or internally. The implant unit can be activated using wifi, RF, IR or Bluetooth technologies.

Implant electrodes e may be spaced apart by about a distance of about 0.2 mm to 40 mm. In other embodiments, the electrodes may be spaced apart by a distance of approximately up to 12 mm. In accordance with yet an example, the distance may be approximately 0.5-7 mm measured between the internal edges of the electrodes. To protect the antenna, electrodes, circuit components, and connecting wires from the environment within a patient's body, implant may include a protective coating that encapsulates the implant 170. In some embodiments, the protective coating may be made from a flexible material to enable bending thereof, such as silicone. The encapsulation material of the protective coating may also resist humidity penetration and protect against corrosion. The surgical implant is substantially sealed and

impervious to fluid. The term "substantially sealed implant" as used herein refers to the condition of having a sufficiently low unintended leakage and permeation rate under given fluid flow or pressure conditions. It will be appreciated that the first pair of electrodes and the second pair of electrodes may be partially covered at their periphery with the encapsulating material, having at least a portion thereof exposed however sealing the implant such that no fluid will enter or exit through the seal surrounding the open window of the electrodes. For example, the first pair of electrodes and the second pair of electrodes are partially embedded within the encapsulating material and comprise an outer layer of encapsulating material extending thereover and leaving at least a portion thereof exposed to the environment.

As seen in Fig. 1A, each one of the two connecting members is constituted by two parallelly extending arched elongated elements 136A and 136B, each extending at an angle and hingedly from the central body 120, such that the connecting members are integrally formed with and extend from the central body portion, allowing for at least one degree of freedom, as will be discussed. Such a connecting member may be through a hinge which may be a living hinge, integral hinge, segmented hinge, etc. The arched elongated segments extend from the side edge 125 and project above the top side 122 of the central body portion 120, as best seen in Fig. 1C, with the wing portions 132A and 132B, each integrally formed with and extending from the opposite ends of the elongated segments. These elongated segments in accordance with the example, house the connecting wires W extending from the components contained in the central body portion to the respective electrodes e disposed on the wing portions 132A and 132B. The wires are provided in a configuration that will allow their deformation without disconnection from the main body or the electrodes. For example, the wire may be in excess, e.g. undulation, coiled etc. It will be appreciated, that while in the exemplified implant 100, each connecting member comprises two separate segments, in accordance with the disclosed subject matter, the connecting member may be a single segment. In accordance with another example, the two separate members may be connected with a connecting layer therebetween, either continuously, leaving no opening between the arched elongated segments, or with a non-continuous, layer, interconnecting the segments.

As further seen in Fig. 1C, each one of the two wing portions is integrally articulated to the respective elongated segments (extension members) extending between the central body portion and the two wing portions.

The connecting member may be a flexible element configured to deform in at least one direction. The connecting member can be of a unitary thickness or as exemplified and best seen in Fig. 1C of thickness decreasing from the portion closest to the area of connection with the central body designated H to thickness designated h at the portion closer to the wing portions. The decrease in thickness can be gradual (as shown) or alternatively provided in segments. Such decrease in thickness provides for flexibility of the connecting members and allows for degrees of freedom both to the connecting members and the movement of the wing portions. The connecting members are configured to endure strain, particularly due to being bent, folded, or stretched, without breaking or suffering permanent injury. "Flexible" as used herein may or may not include the further properties of being resilient or elastic. Deformation could refer to at least one parameter change, e.g. change of length, thickness etc. in a pre-specified space.

The connecting members allow several degrees of freedom to the two wing portions as best illustrated in Figs. 1B and IC. The connecting members are configured with flexibility along the length thereof and at least at points designated C, B and A, where point C designates the section at the connection of the elongated segment to the central body portion, point B designates the segment at around the center of the arch of the elongated member and point A designates the segment integrally connecting the elongated members to the wing portions. Thus as seen in Fig. IC at point B the elongated segment is allowed to deform and open the arch and move the wing portion at an angle  $\alpha$  which can be between 0 degrees and up to 180 degrees. In other examples, the angle  $\alpha$  can extend between -90 (e.g. in a direction towards the bottom side 124) to 270 degrees, or as shown at about 30 degrees. The wing portion can pivot at point A at angle  $\beta$  which can be between 0 degrees to about 100 degrees. In other examples, the angle can extend between -90 (e.g. towards the bottom side 124) to 100 degrees, or as illustrated up to 25 degrees. It will be appreciated that while the angular displacement has been shown separately for each of the points a combination of displacement is allowed and the wing portions can be angled in combination with the angular or other deformation of the connecting members. In accordance with disclosed subject matter and illustrated example, 0 degrees is the resting position of the element which has the degree of freedom to change position(s).

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As further seen in Fig 1B, the wing portions can be displaced in the direction of arrow X (e.g. horizontally), arrow Z (vertically) or arrow Y (angularly, e.g. inwards the central portion or outwardly therefrom, where the wing portions can flex towards or away from each other). Such flexibility along multitude of dimensions, allow positioning of the implant and in particular its wing portions over the treated muscle, in a saddle like position and conform to the dimensions of the muscle, which may be different from subject to subject. The disposition of the wing portion is further defined by angle  $\beta$  which provide for an angle between the edge 137 of the wing and the horizontal plane extending through the central body portion. The angle  $\beta$  can be between about 0 degrees to 10 degrees, and in the illustrated example is between 3 to 7 degrees.

As already discussed, the surgical implant may be formed from a unitary elastomeric material. To allow anchoring of the implant in its designated position the implant may be provided with anchoring arrangements. In the disclosed example, the anchoring arrangement is in the form of suturing holes (e.g. 152, 155). As the implant is made of an elastomeric material, to reinforce the suturing holes, the implant may be provided with anchoring elements made of a material configured to withstand the forces acting on the implant and the sutures, e.g. during the tongue movement. Such a material can be e.g. a PEEK, ceramic, titanium etc.

As seen in Fig. 1B the suturing holes 152 can be provided at the wing portions at the desired location. In addition, other anchoring elements can be provided at the central body portion, e.g. adjacent the edges thereof as seen in Fig. 1D designated as 154. It will be appreciated that other configurations for anchoring the implant are envisioned and while for example the central body portion comprises four such holes, only few or none of these can be provided. In addition, the positioning of the suture holes on the wing portions as illustrated in the accompanying drawings are for illustration purposes only and other shapes, configurations and positions thereof are envisioned. Other types of anchoring arrangements are envisioned, such as adhesives, staples etc, as disclosed herein.

The central body portion can further be provided with a load bearing reinforcing structure 158, internally disposed, and configured to provide structural rigidity to the central body portion. The reinforcing structure can be resilient and allow for a degree of flexibility to the central body portion when force is applied thereto in the direction of arrow E, allowing at least a portion of the central body portion to flex e.g. as seen in Fig. 1B. the reinforcing structure in the illustrated example is provided through the central body and provides for a walled structured

156 to surround the electronics 160 and also longitudinal ribs 158 as seen e.g. in Fig. IA. It will be appreciated the the reinforcing structure may have a different structure, e.g. crossed ribs to form a net like structure, a spiral, e.g. interconnected stips, etc. to provide for the same function of reinforcement and substantial exposure of the antenna a and the electronic parts.

5 The implant may further comprise a surgical mesh, e.g. polymeric mesh, provided at least over a portion thereof. In another example, the surgical mesh may be of any suitable material.

10 In another aspect of the disclosed subject matter there is disclosed an implant unit activation device illustrated in Figures 4 to 7C and generally designated 200. The device, comprises a main body 220 comprising an implant activator and an axially displaceable retractor 240 configured to displace relative the main body.

15 The implant activator comprises an antenna, a power source and associated circuitry (not shown) and being configured to wirelessly transfer energy from the power source to an implant unit (e.g. surgical implant 100) during implantation of the implant unit into the body of a subject to cause stimulation of at least one nerve in the body of the subject during the implantation procedure. The axial displacement of the retractor 240 allows adjusting of the degree of energy received by the implant unit. The activation device is configured to deliver energy to the implant unit with the retractor allowing to displace or more particularly retract the activation unit in the direction of arrow P (seen in Fig.7A) from the implant so as to control the amount of energy received by the implant unit as a function of distance at which it is delivered thereto. As an alternative example, the axis of displacement may comprise e.g. displacement along axis Q and\or R (e.g. as shown in Figs. 6 and 7A).

20 The retractor 240 is in this example a sleeve like member configured to controllably slide over the main shaft S of the activation device main body. The sleeve like member defines a hollowed and axially extending interior which securably mounts over the shaft of the main body. To facilitate the retraction, the sleeve like member is provided with a release lever 245 and engagement mechanism 250, such that the engagement mechanism is configured to selectively engage the corresponding engaging members 225 on the shaft of the main body. In the present example the shaft is provided with toothed surface 225 and the inner side of the sleeve is provided with the engagement mechanism 255 constituted by a protrusion configured to engage the toothed surface to lock

thereagainst. The main body shaft may be provided with indicia 235 allowing the user to determine the location at which it is desired to lock the sleeve against the shaft. As seen in Fig. 4, the shaft is provided with a protrusion 229 which when aligned with the sleeve extends slidably in a slit 243 in the sleeve which in the example extends at two opposite sides of the sleeve as seen in Fig. 5. It will be appreciated that other configurations are envisioned that will allow the main body of the activation device to be distanced from the implant unit keeping the device at the predetermined position with respect to the implant unit. The sleeve can further be provided with a support and gripping element 247 to allow the user to grip the sleeve, while activating the lever 245 to release the engagement of the mechanism 255 and retracting the shaft body through the sleeve to distance its end portion 223 from the opening 241 in the sleeve.

As seen in the illustrated example, the edge of the device 200 is angled to enable line of sight during use and for ergonomic considerations. It will be appreciated, that while in the illustrated example the amount of energy or power level is determined by the axial movement of the retractor, other examples include a screw on sleeve, partial elements extending from the shaft and configured to distance the edge of the shaft from the point of contact with the implant device. In an alternative example, the amount and level of energy may be controlled directly through the device, without adjusting the distance between the shaft edge relative the implant device.

An exemplary method of positioning and activating a neurostimulation implant device (e.g. surgical implant 100) in accordance with the disclosed subject matter is provided. The method in accordance with the disclosed subject matter , comprises:

providing the implant and positioning it over the tissue of the subject, e.g. the genioglossus muscle.

providing an implant unit activation device as disclosed, the device comprising: a main body comprising an implant activator having a power source, a second antenna configured to provide a signal to the first antenna and an axially displaceable adaptor\retractor associated with the implant activator, the implant activator configured to wirelessly transfer energy from a power source to the implant during implantation to cause modulation of at least one nerve in the body of the subject; and

wherein the axial displacement (e.g. retraction) of the adaptor from at least a first position to at least a second position allows adjusting of the degree of energy received by the implant unit.

To determine the correct location for positioning the implant and in particular the electrodes to stimulate the nerve, next stem comprises identifying the stimulation threshold by determining a degree of nerve modulation response for each of the at least first pair of electrodes and a second pair of electrodes by positioning said first pair of electrodes at an estimated implant location proximal to the nerve and selectively displacing the second antenna to deliver a first amount of power and a second amount of power required to obtain a stimulation threshold in at least the first pair of electrodes based on one or more patient signals;

positioning the at least the second pair of electrodes at an estimated location and delivering the second amount of power required and determining a degree of nerve

modulation by the at least said second pair of electrodes.

wherein the stimulation threshold is based, at least in part on at least one neuromuscular response during stimulation of each electrode of the at least a first pair of electrodes and a second pair of electrodes.

In one embodiment the implant may be configured for treatment of obstructive

sleep apnea and the location of implantation may be in the vicinity of the hypoglossal nerve. In accordance with this embodiment the neurostimulation device may be configured to modulate at least one branch of the hypoglossal nerves.

The second amount may be greater or equal to the first amount of power.

The second amount may be equal to or less relative the first amount of power.

Claims

1. A surgical implant comprising:
  - a. a substantially planar central body portion having a top side and a bottom side;
  - b. at least two adjustable wing portions, each of the at least two adjustable wing portions including one or more electrodes for emitting an electrical field;
  - c. at least two connecting members, each one of the at least two connecting members extending from opposite sides of the central body portion, the each one of the at least two connecting members being configured for flexibly connecting each one of the at least two wing portions at opposite sides to said central body portion, wherein the central body portion is further provided with an internally disposed load bearing reinforcing structure, configured to provide structural rigidity to the central body portion, and wherein the wing portions are more flexible than the central body portion.
2. A surgical implant in accordance with Claim 1, wherein each one of said at least two connecting members extend from the central body through at least one hinge member.
3. A surgical implant in accordance with Claim 1, wherein the connecting member is a flexible element configured to deform in at least one direction, wherein the flexible element is optionally in the form of a flexible arch permitting bending movement along its length in a first direction such that the central body and each of the at least two wing portions flex away from each other.
4. A surgical implant in accordance with Claim 1, comprising a flexible arch the flexible arch including:

at least one central segment arranged along the length of the flexible arch; and

at least two hinge structures, each one of the hinge structures being disposed between the central body and the at least one central segment and the one of the at least two wing portions and the central segment and oriented in a direction transverse to the length of the central segment.
5. A surgical implant in accordance with Claim 3 or Claim 4, wherein the flexible arch is formed from a unitary elastomeric material and the hinges comprise living hinges; or wherein

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the flexible arch is formed from multiple segments; the multiple segments being connected through living hinges.

6. A surgical implant in accordance with any one of Claims 3 to 5 , wherein the flexible arch has a narrowing width, having the largest width at the area of connection to the central body and a narrower width at the area of connection with at least one of the wing portions.

7. A surgical implant in accordance with Claim 1, wherein the surgical implant is formed from a unitary elastomeric material.

8. A surgical implant in accordance with any one of the above Claims, wherein the surgical implant includes at least one anchoring arrangement, the at least one anchoring arrangement comprising an embedded reinforcing element and/or a reinforcing layer of material forming part of the arrangement.

9. A surgical implant in accordance with Claim 8, wherein the reinforcing layer of material is a mesh material.

10. A surgical implant in accordance with any one of the above Claims, wherein the at least two wing portions have at least one degree of freedom and are flexibly adjustable to various angular dispositions with respect to the main body, and wherein the angular dispositions are between about -90 to up to 270 degrees;

11. A surgical implant in accordance with any one of the above Claims, wherein the at least two wing portions are flexibly adjustable to various angular dispositions along more than one axis.

12. A surgical implant in accordance with Claim 11, wherein the at least two wing portions are flexibly adjustable to various angular dispositions along and/or around three axis.

13. A surgical implant in accordance with Claim 11, wherein the at least two wing portions have more than three degrees of freedom and are flexibly adjustable to various angular dispositions with respect to the main body and/or the connecting members.

14. A surgical implant in accordance with Claim 1, wherein at least in one configuration of the implant device, the connecting member comprises a flexible arch which protrudes beyond the top side of the substantially planar surface of the central body.

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15. A surgical implant in accordance with any one of the above Claims, wherein the central body portion is provided with an antenna configured to receive a signal and wherein each one of the at least two wing portions is provided with at least a pair of electrodes in electric communication with the antenna, the electrodes being configured to receive an electric current in response to the signal received by the antenna, such that at least one of pair of electrodes is configured to emit an electrical field.
16. A surgical implant in accordance with Claim 15, wherein the first pair of electrodes and the second pair of electrodes is partially covered at their periphery with the encapsulating material, having at least a portion thereof exposed.
17. A surgical implant in accordance with Claim 15 or Claim 16, wherein the surgical implant is configured to conform to an exterior surface of a genioglossus muscle of a subject, such that the at least two wing portions are positioned at the sides of the genioglossus muscle adjacent to terminal fibers of a medial branch of a hypoglossal nerve, and wherein the electrodes generate electric field sufficient to modulate the terminal fibers of a medial branch, when spaced apart thereof.
18. A surgical implant in accordance with any one of Claims 15 to 17, wherein at least one of the first pair of electrodes and the second pair of electrodes are connected to electric circuitry through wires, the circuitry being disposed on the central body and the wires being configured to extend through the respective connecting members.
19. A surgical implant according to any of the above claims in combination with an implant unit activation device, the implant unit activation device comprising: a main body comprising an implant activator and an axially displaceable adaptor configured to displace relative the main body, the implant activator having a power source and being configured to wirelessly transfer energy from the power source to the surgical implant during implantation of the surgical implant into the body of a subject to cause stimulation of at least one nerve in the body of the subject; and wherein the axial displacement of the adaptor allows adjusting of the amount of energy received by the surgical implant.
20. A method of positioning and activating a surgical implant, the method comprising providing a surgical implant according any one of the above claims, wherein the surgical implant is a neurostimulation device; and wherein:

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the central body portion of the surgical implant is provided with a first antenna configured to receive a signal;

the surgical implant has at least a first pair of electrodes and a second pair of electrodes operatively coupled to the central body portion;

the central body portion is in electric communication with at least the first pair of electrodes and the second pair of electrodes, said at least first pair of electrodes and the second pair of electrodes being configured to receive an electric signal in response to the signal received by the first antenna, such that at least one of pair of electrodes is configured to emit an electrical field to stimulate a nerve in a subject's body;

the method further comprising:

providing an implant unit activation device, the implant unit activation device comprising: a main body comprising an implant activator having a power source, a second antenna configured to provide a signal to the first antenna and an axially displaceable adaptor associated with the implant activator, the implant activator configured to wirelessly transfer energy from a power source to the neurostimulation device during implantation to cause modulation of at least one nerve in the body of the subject; and

wherein the axial displacement of the adaptor from at least a first position to at least a second position allows adjusting of the amount of energy received by the implant unit;

identifying the stimulation threshold by determining a degree of nerve modulation response for each of the at least first pair of electrodes and a second pair of electrodes by positioning said first pair of electrodes at an estimated implant location proximal to the nerve and selectively displacing the second antenna to deliver a first amount of power and a second amount of power required to obtain a stimulation threshold in at least the first pair of electrodes based on one or more patient signals;

positioning the at least the second pair of electrodes at an estimated location and delivering the second amount of power required and determining a degree of nerve modulation by the at least said second pair of electrodes.

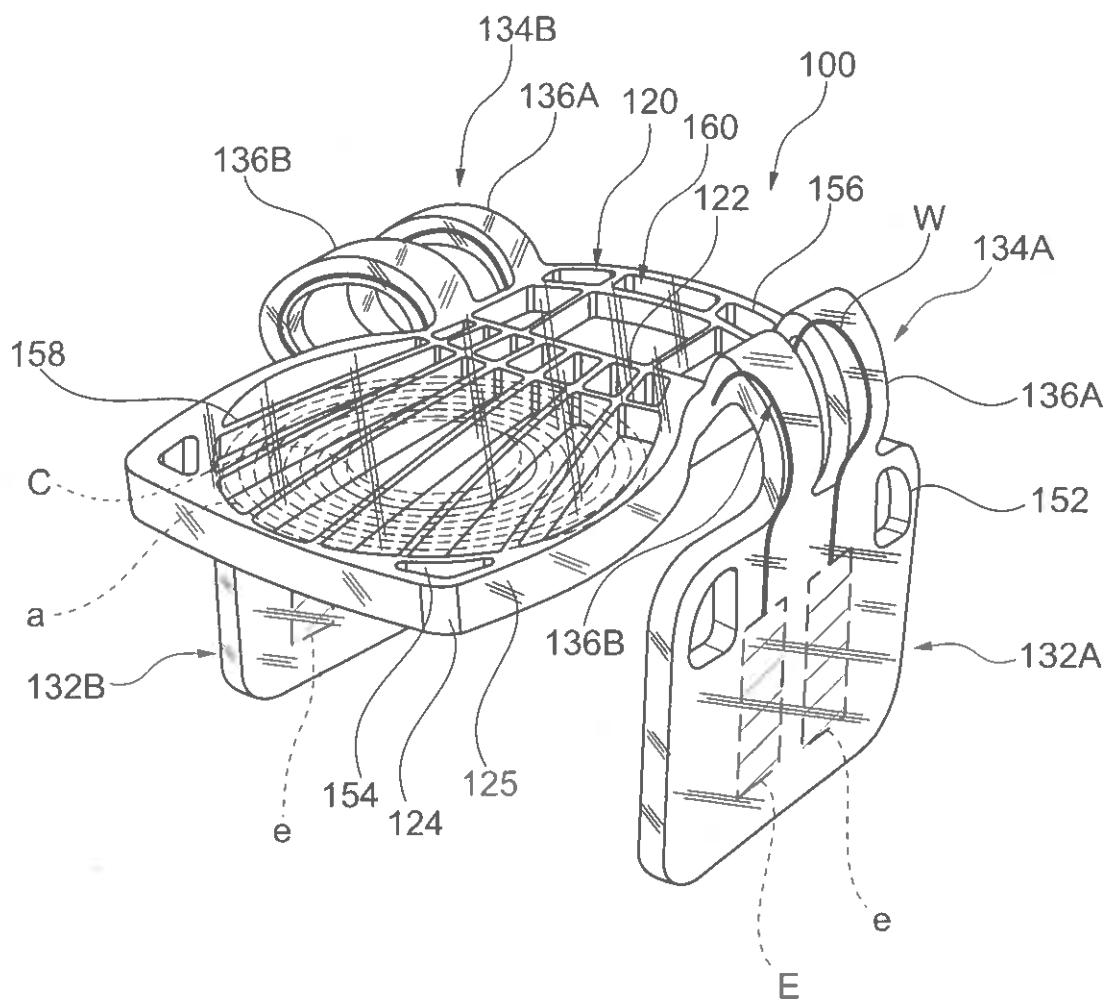


Fig. 1A

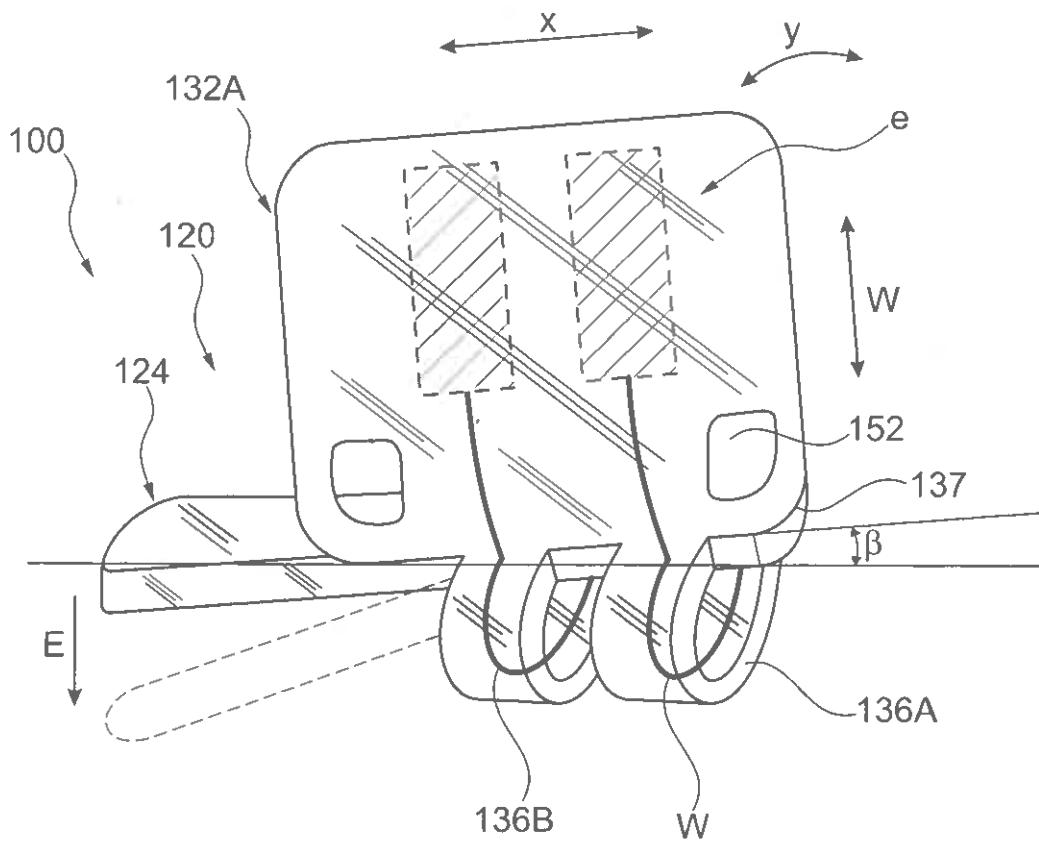


Fig. 1B

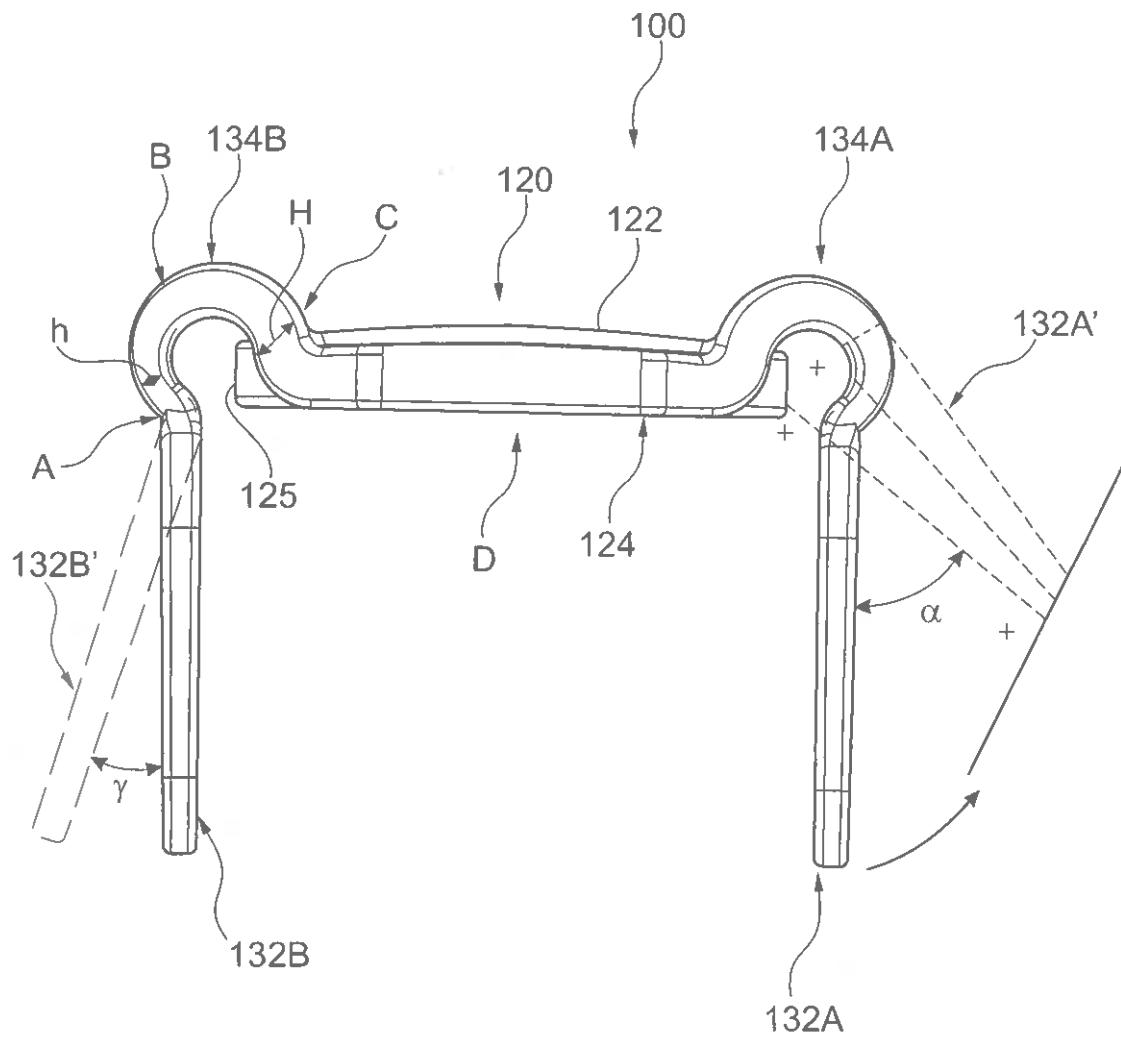


Fig. 1C

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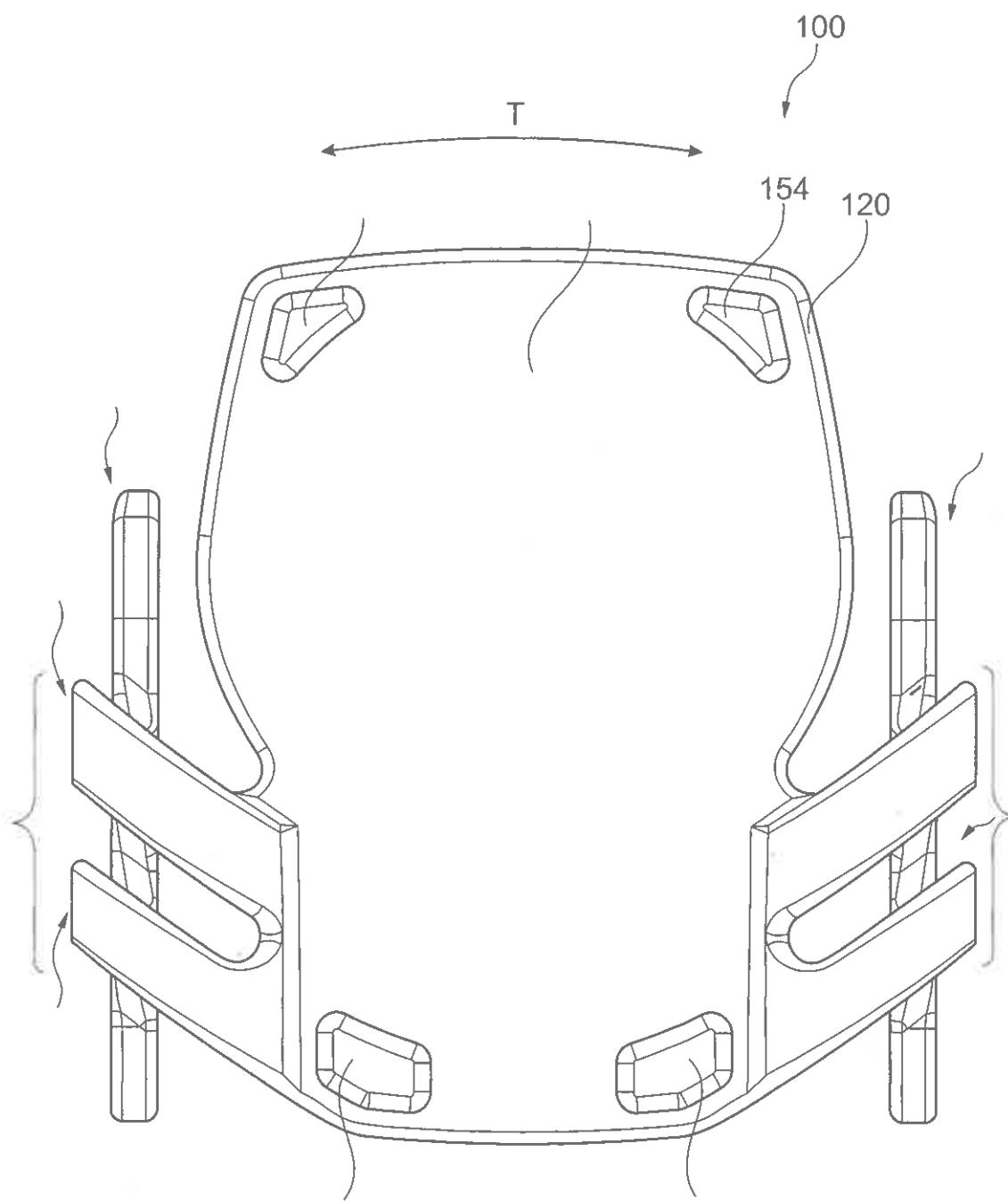


Fig. 1D

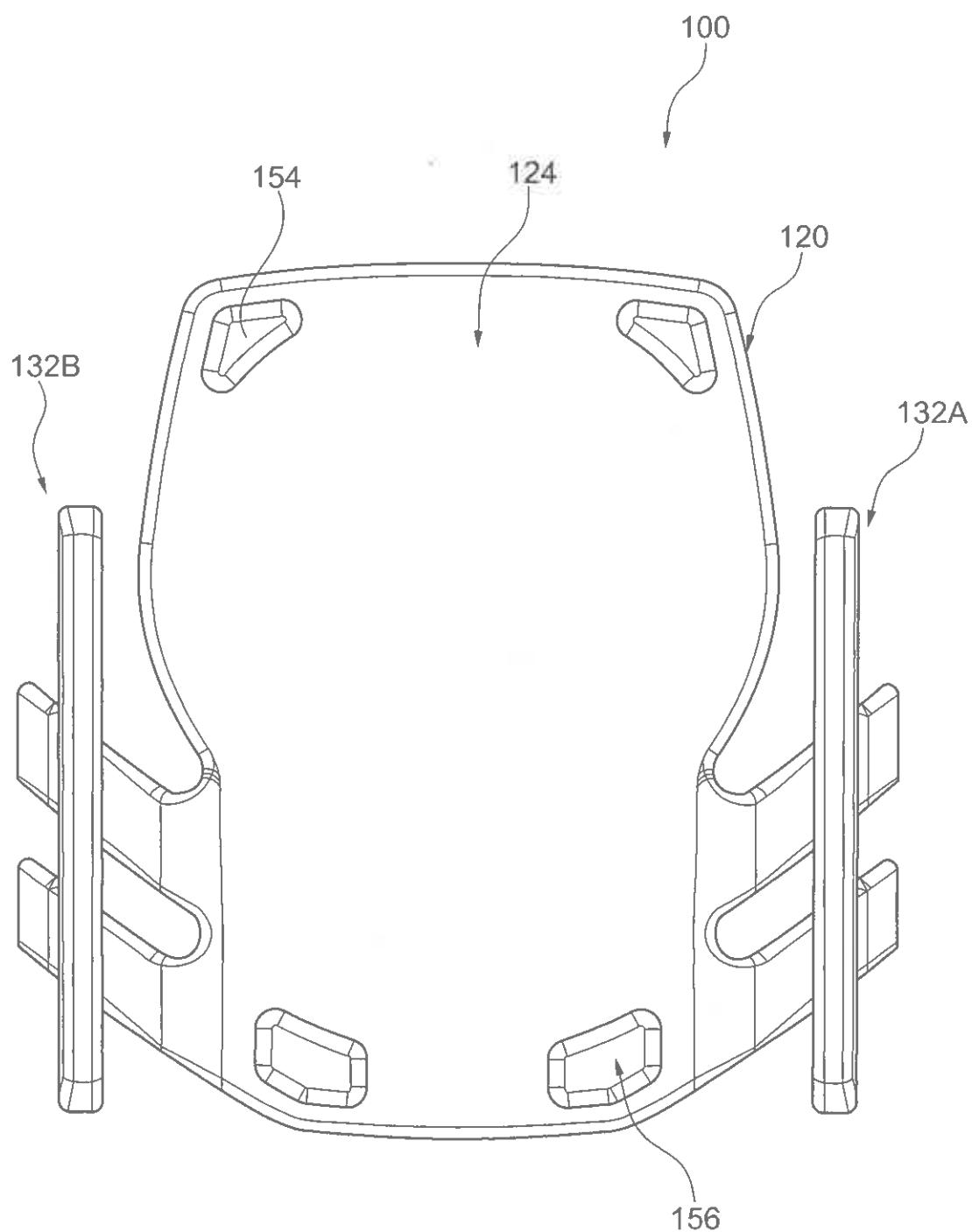


Fig. 1E

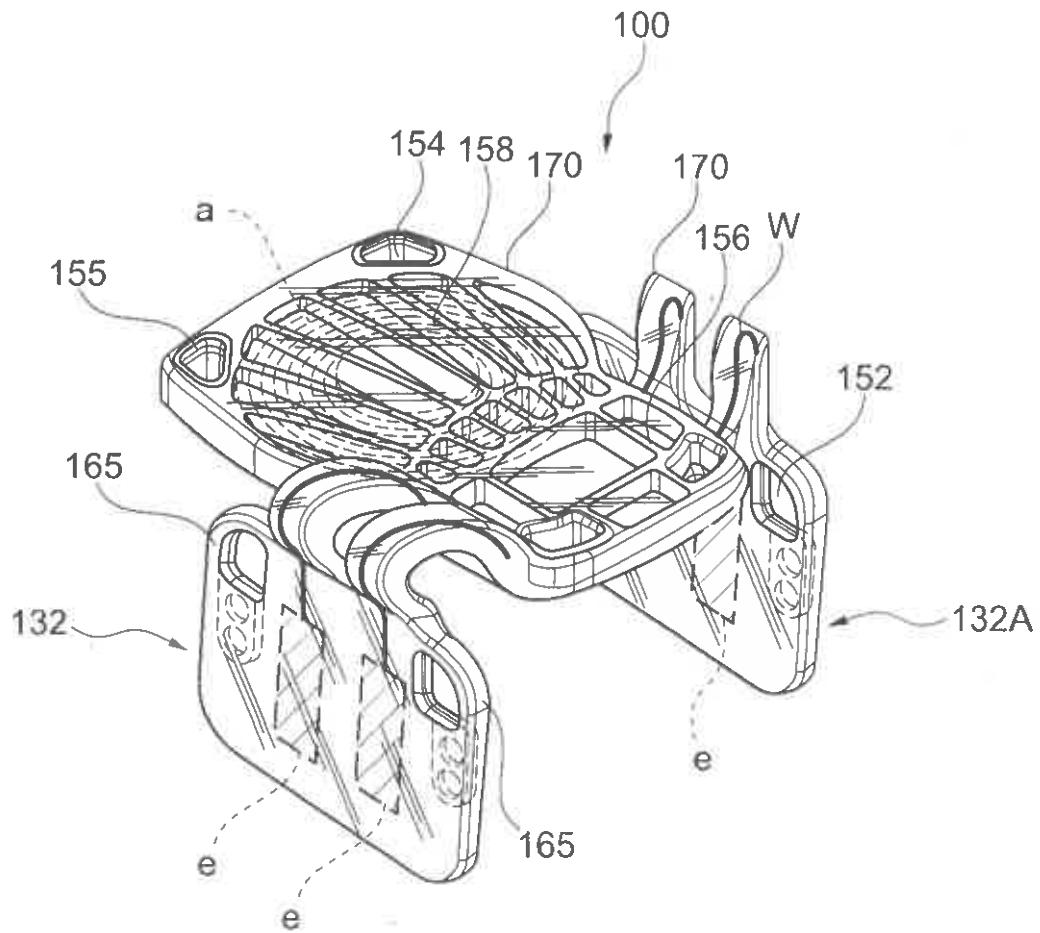


Fig. 2

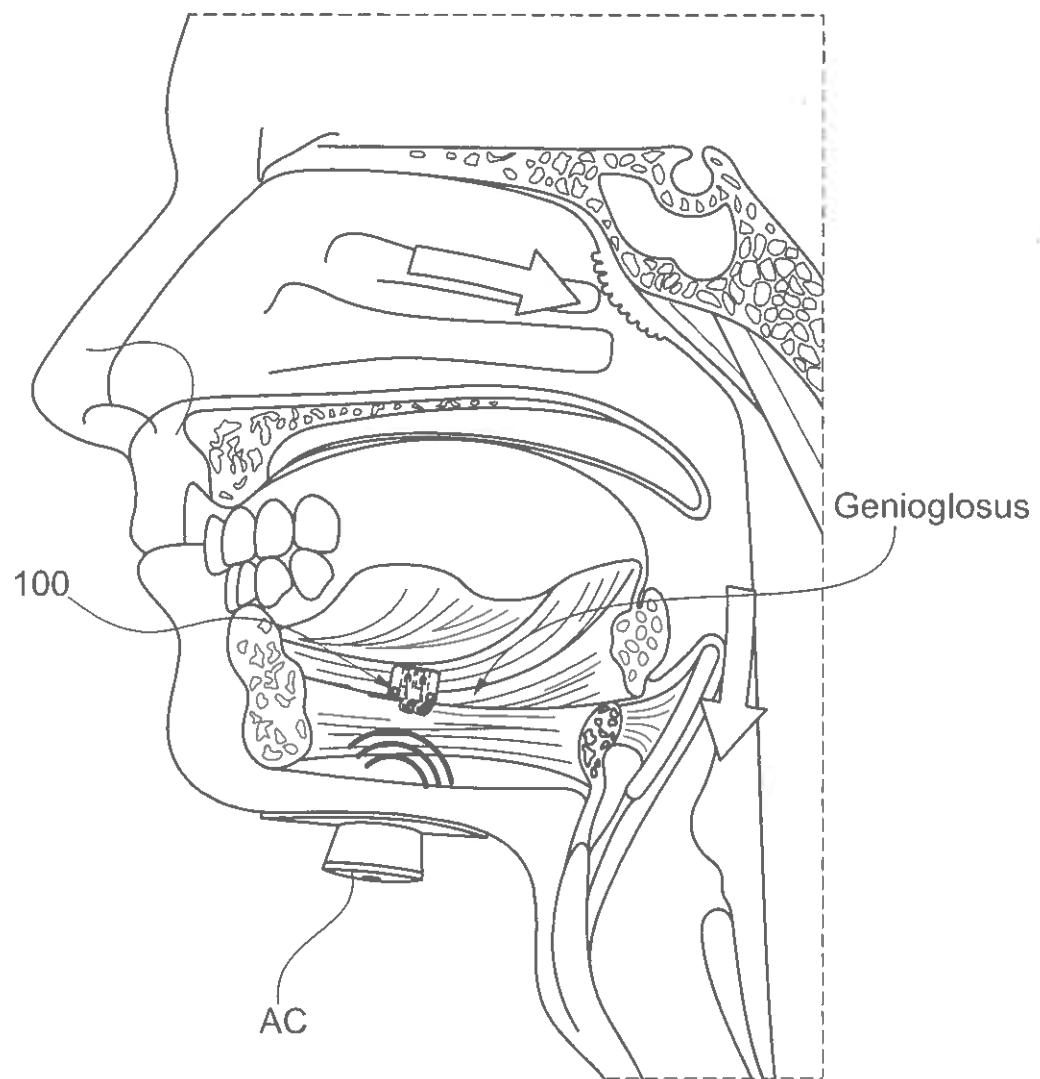


Fig. 3

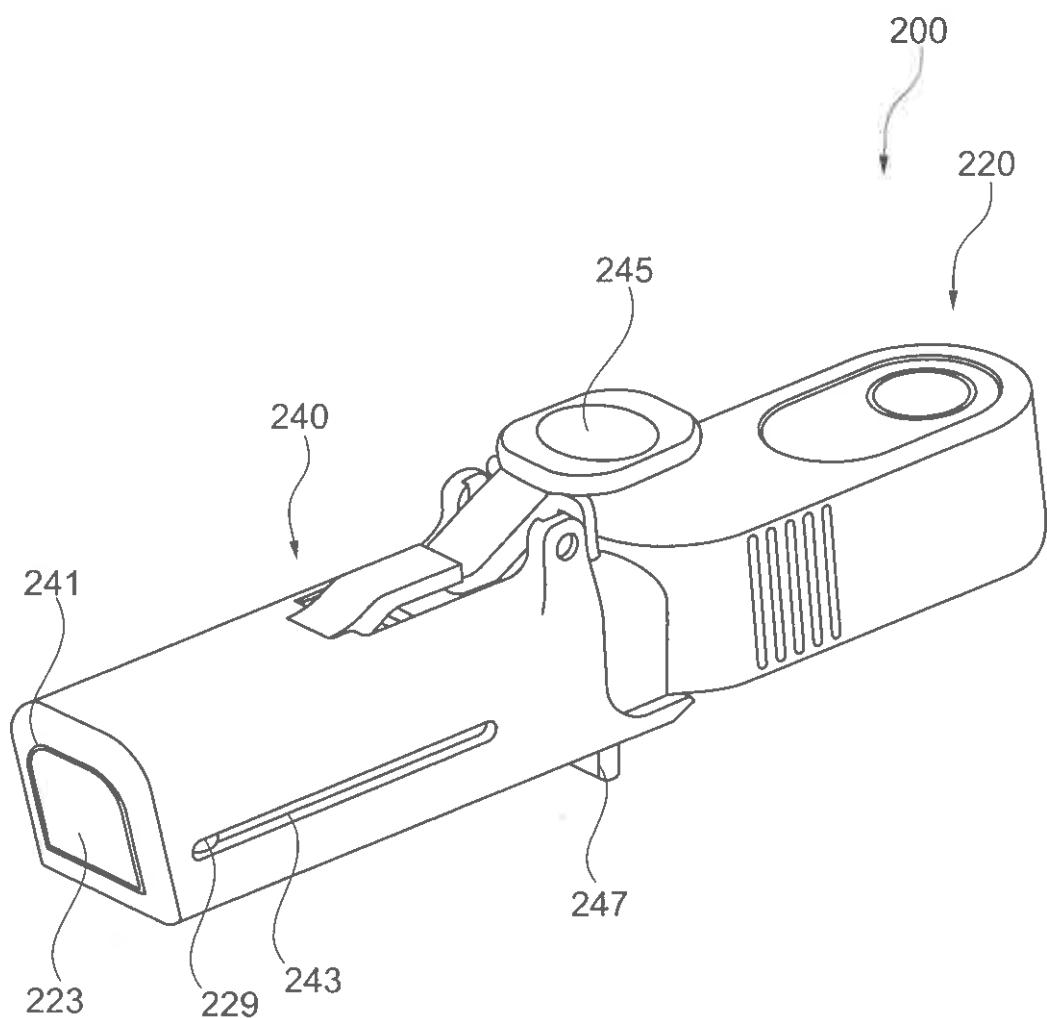


Fig. 4

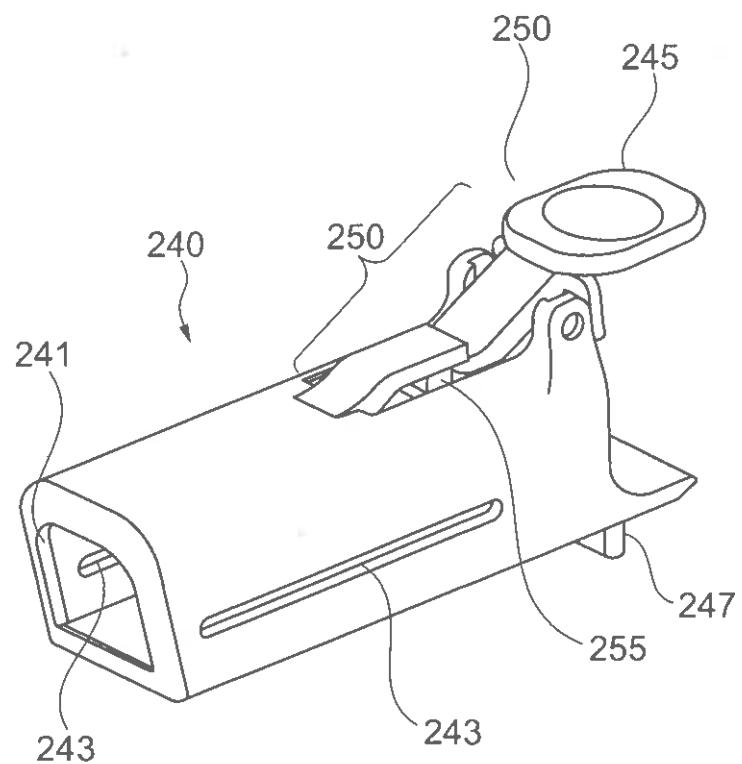


Fig. 5

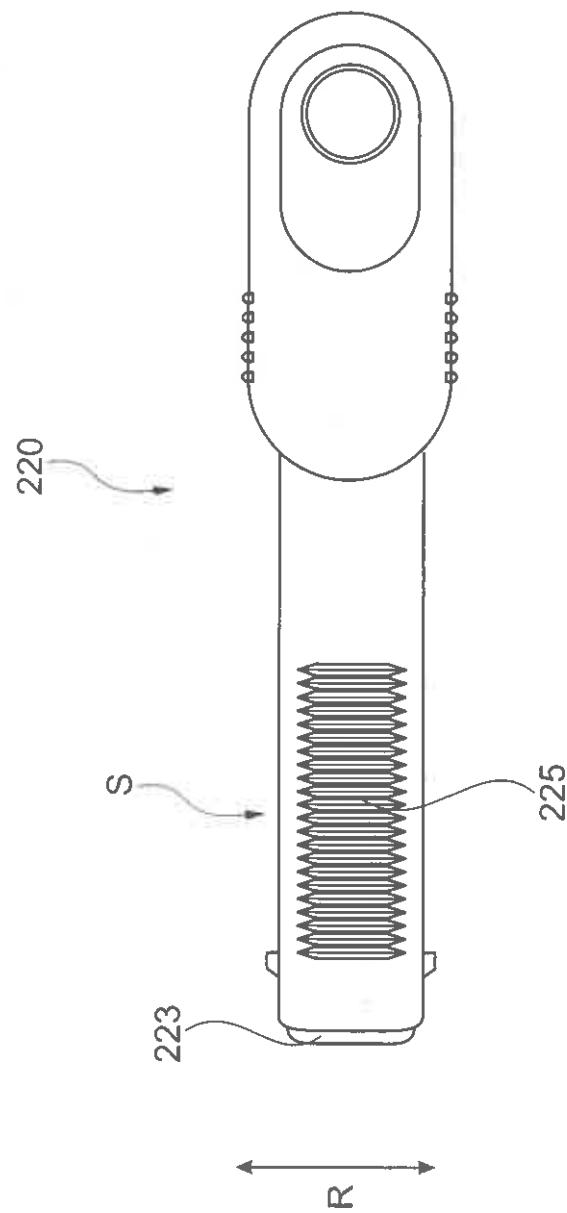


Fig. 6

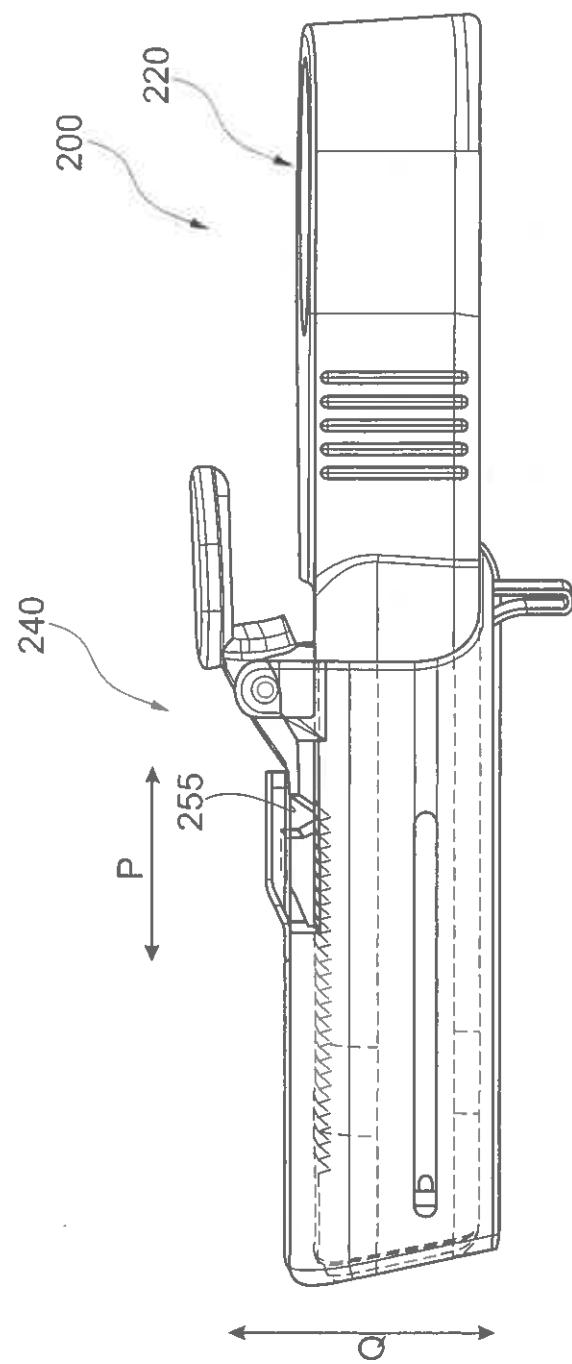


Fig. 7A

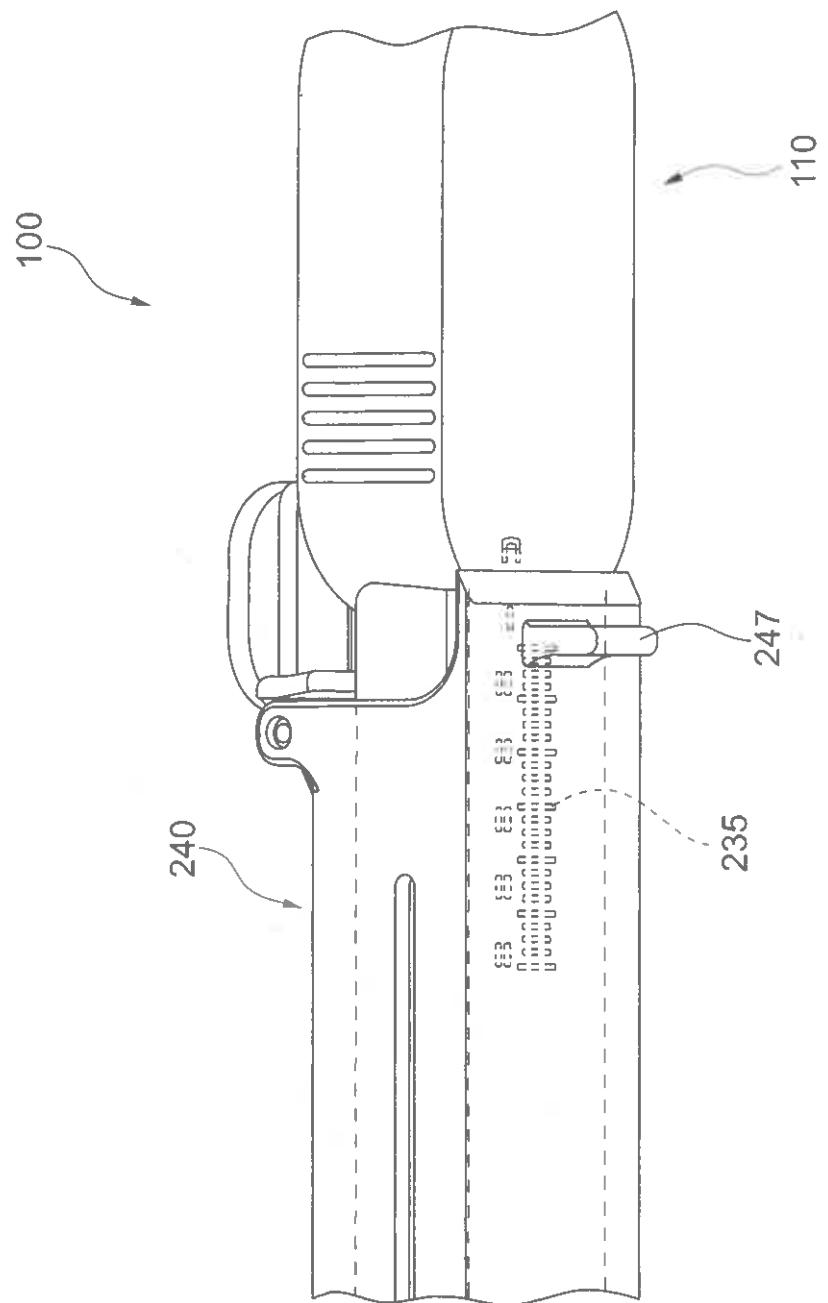


Fig. 7B

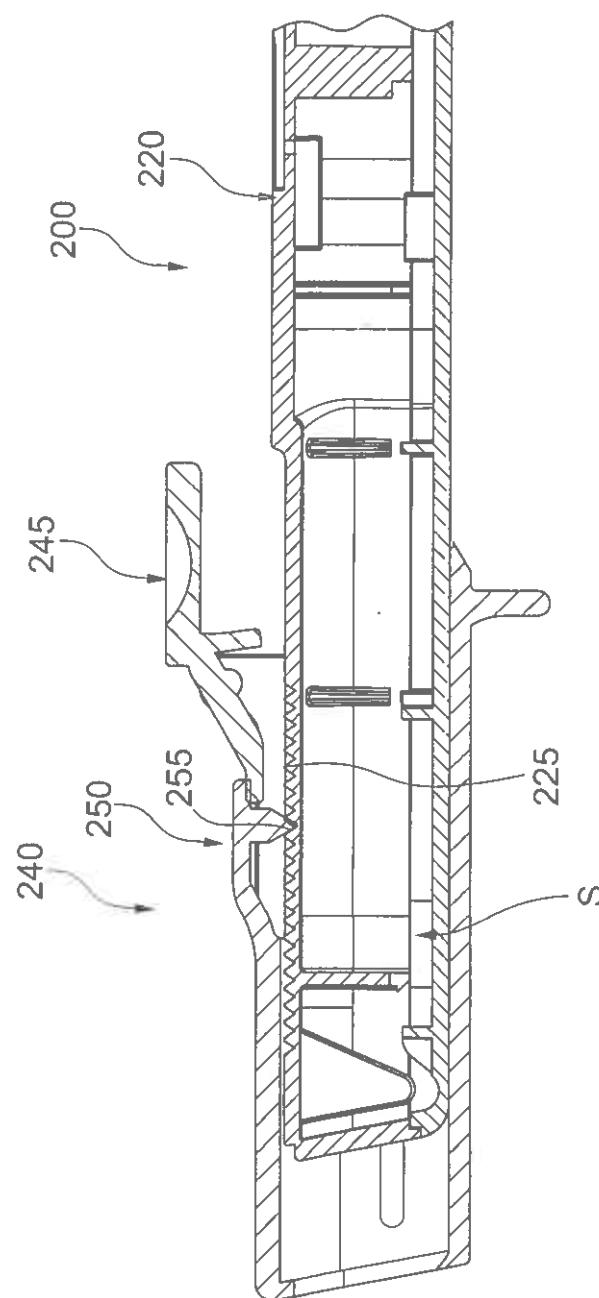


Fig. 7C