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(19) **United States**(12) **Patent Application Publication****Jang**(10) **Pub. No.: US 2004/0267239 A1**(43) **Pub. Date: Dec. 30, 2004**(54) **CATHETER SYSTEM HAVING A BALLOON ANGIOPLASTY DEVICE DISPOSED OVER A WORK ELEMENT LUMEN**(75) Inventor: **Yue-Teh Jang**, Fremont, CA (US)

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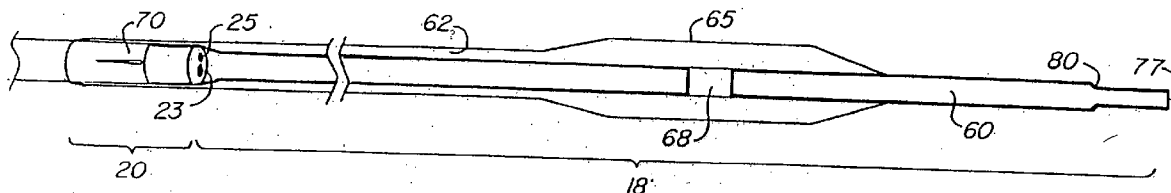
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May 21, 1997, now Pat. No. 5,941,870, which is a continuation of application No. 08/504,363, filed on Jul. 19, 1995, now abandoned, which is a continuation of application No. 08/291,215, filed on Aug. 16, 1994, now abandoned, which is a continuation of application No. 08/100,642, filed on Jul. 30, 1993, now Pat. No. 5,364,347, which is a continuation of application No. 07/975,752, filed on Nov. 13, 1992, now abandoned.

**Publication Classification**(73) Assignee: **Cardiovascular Imaging Systems, Inc.**(21) Appl. No.: **10/778,988**(22) Filed: **Feb. 13, 2004**(51) **Int. Cl.<sup>7</sup> ..... A61M 31/00; A61B 8/12**(52) **U.S. Cl. .... 604/509; 600/439; 600/467**(57) **ABSTRACT****Related U.S. Application Data**

(63) Continuation of application No. 09/779,128, filed on Feb. 7, 2001, now Pat. No. 6,712,783, which is a continuation of application No. 09/379,930, filed on Aug. 23, 1999, now Pat. No. 6,264,632, which is a continuation of application No. 08/861,397, filed on

An intravascular catheter system has a balloon angioplasty device disposed about a common lumen near its distal end. The common lumen is in communication with multiple lumens within a proximal region of the catheter body to allow for positioning of the catheter over a movable guide wire and convenient delivery of imaging or interventional devices to a desired region of the blood vessel being treated.



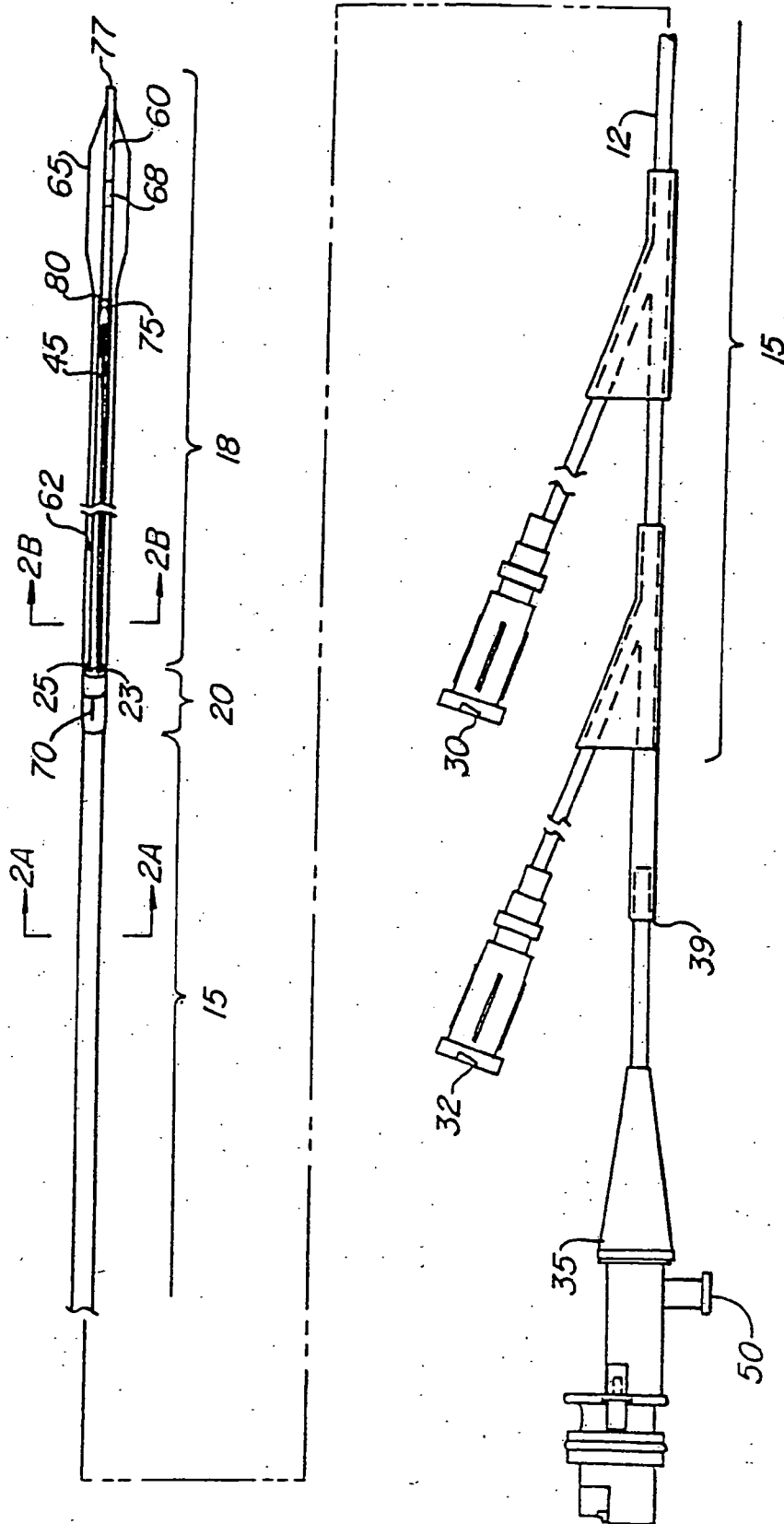


FIG. 1.

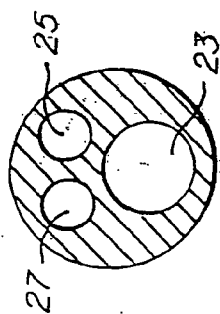


FIG. 2A.

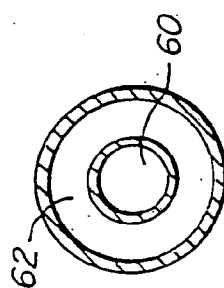


FIG. 2B.

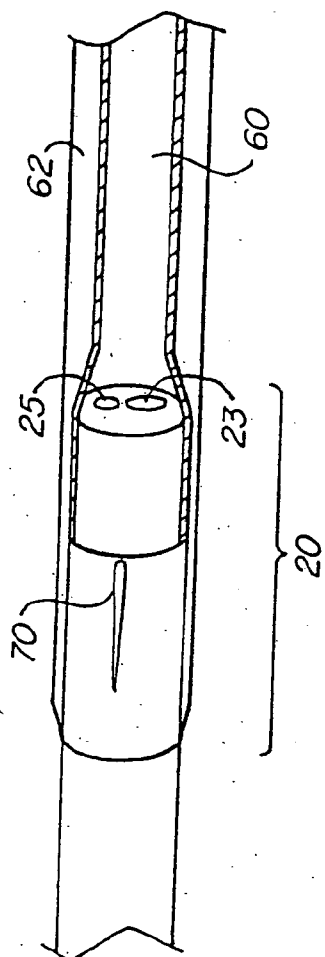


FIG. 3.

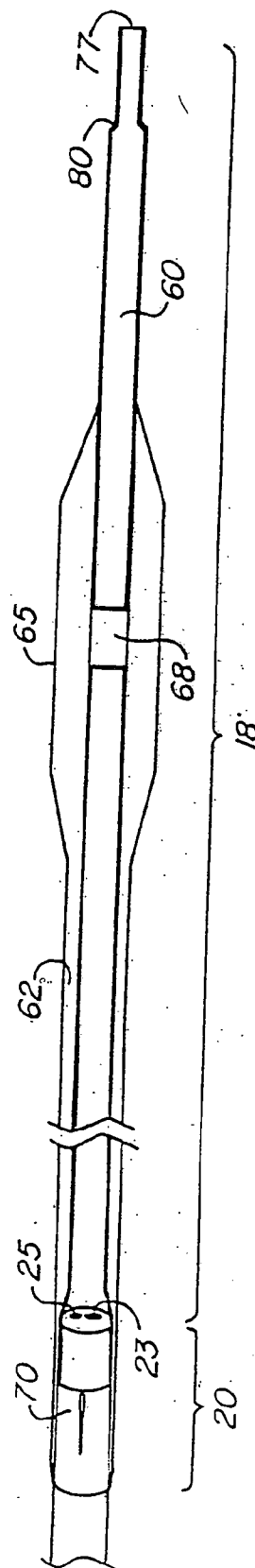


FIG. 4.

## **CATHETER SYSTEM HAVING A BALLOON ANGIOPLASTY DEVICE DISPOSED OVER A WORK ELEMENT LUMEN**

### **CROSS REFERENCE TO RELATED APPLICATIONS**

[0001] The present application is a continuation of co-pending U.S. patent application Ser. No. 09/379,930, filed on Aug. 23, 1999, which is a continuation of U.S. patent application Ser. No. 08/861,397, filed on May 21, 1997, now U.S. Pat. No. 5,941,870, which is a continuation of U.S. application Ser. No. 08/504,363, filed on Jul. 19, 1995, now abandoned, which is a continuation of U.S. application Ser. No. 08/291,215, filed on August 16, 1994, now abandoned, which is a continuation of U.S. application Ser. No. 08/100,642, filed on Jul. 30, 1993, now U.S. Pat. No. 5,364,347, which is a continuation of U.S. application Ser. No. 07/975,752, filed on Nov. 13, 1992, now abandoned. The priority of these prior applications is expressly claimed and their disclosures are hereby incorporated by reference in their entirety.

### **BACKGROUND OF THE INVENTION**

#### **[0002] 1. Field of the Invention**

[0003] The present invention relates generally to catheter systems for imaging and treatment of stenoses within a patient's vascular system and more particularly to a catheter system in which a balloon angioplasty device can be delivered along with an imaging or interventional work element to a desired region within a blood vessel.

#### **[0004] 2. Description of the Background Art**

[0005] Arteriosclerosis, also known as atherosclerosis, is a common human ailment arising from the deposition of fatty-like substances, referred to as atheroma or plaque, on the walls of blood vessels. Such deposits occur both in peripheral blood vessels that feed limbs of the body and coronary blood vessels that feed the heart. Localized accumulation of deposits within regions of the blood vessels may result in stenosis, or narrowing of the vascular channel. When this occurs, blood flow is restricted and the person's health is at serious risk.

[0006] Numerous approaches for reducing and removing such vascular deposits have been proposed, including balloon angioplasty, in which a balloon-tipped catheter is used to dilate a stenosed region within the blood vessel; atherectomy, in which a blade or other cutting element is used to sever and remove the stenotic material; laser angioplasty, in which laser energy is used to ablate at least a portion of the stenotic material; and the like.

[0007] In order to apply such intervention techniques more effectively, a variety of vascular imaging devices and methods may be employed. Of particular interest to the present invention, imaging catheters having ultrasonic transducers at their distal ends have been employed to produce images of the stenotic region from within the blood vessel. A number of specific designs for ultrasonic imaging catheters have been described. An early design is illustrated in U.S. Pat. No. 4,794,931, where the mechanical components of the imaging system are located within a housing at the distal end of the catheter. The housing includes a fixed guidewire, which is used to position the catheter within the vascular system,

at its distal tip. While the use of such fixed guidewire designs can provide excellent image quality, under some circumstances it is desirable to use an "over the wire" design where the catheter may be introduced over a separate (movable) guidewire. The use of a movable guidewire offers certain advantages, including improved steering capability through narrow regions and easier catheter exchange, e.g., substitution of an interventional catheter for the imaging catheter.

[0008] Exchanging the imaging catheter for an interventional or other catheter within a patient's vascular system is time consuming and may be injurious to the patient. It is desirable therefore to combine imaging and interventional capabilities in a single catheter system. A design for an ultrasonic imaging catheter having a balloon angioplasty device is described in U.S. Pat. No. 5,117,831. One depicted embodiment uses a fixed guidewire and is thus subject to the disadvantages noted above. Another embodiment has a guidewire movable through the ultrasonic imaging transducer and its associated drive shaft. This requires that the transducer and the drive shaft be made hollow and increased in diameter in order to accommodate the guidewire therein. Additionally, the transducer is fixed at the end of the drive shaft and not movable along the length of the catheter.

[0009] To be able to cross very narrow lesions, the diameter of the catheter should be as small as possible at its distal end. Furthermore, the need to move the catheter body within the patient should be minimized. The blood vessel interior is delicate, may be weakened by disease, and is therefore susceptible to injury from movement of the catheter body within it.

[0010] For the reasons stated above, it would be advantageous to provide a catheter capable of delivering a balloon angioplasty system in combination with an imaging or interventional work element to a region of interest within the vascular system. Such delivery should be accomplished with a minimum repositioning of the catheter body within the blood vessel. Additionally, the catheter should be as narrow as possible at its distal end to allow for entry into and through narrow and tortuous regions of the patient's vascular system.

### **SUMMARY OF THE INVENTION**

[0011] The present invention provides a catheter system having the ability to deliver both an angioplasty balloon and another work element for imaging or treating a region within patient's vascular system. The catheter system comprises a catheter body having at least a proximal and a distal region. The proximal region has at least two lumens, one for carrying a movable guidewire and another for carrying a work element. The work element will typically be an ultrasonic imaging transducer but may be another imaging device or even an interventional device for treating the blood vessel in combination with the angioplasty balloon. The distal region of the catheter body has a common lumen connected to and in communication with the two lumens of the proximal region. The angioplasty balloon is disposed about the common lumen of the distal region, and the catheter system further includes an associated means for inflating the balloon, typically an inflation lumen extending from the proximal end of the catheter body to the balloon.

[0012] The catheter of the present invention will allow for the performance of rapid and convenient balloon angioplasty

and imaging or other treatment of the diseased vessel while minimizing the need to reposition the catheter body between procedures. Additionally, the distal end of the catheter will be relatively narrow to allow for movement of the catheter into restricted spaces of the patient's vascular system and particularly into narrow regions and stenoses within the coronary arteries.

#### BRIEF DESCRIPTION OF THE DRAWINGS

[0013] **FIG. 1** depicts a preferred embodiment of a catheter according to the present invention;

[0014] **FIG. 2A** is a cross-sectional view through section line A-A of the catheter depicted in **FIG. 1**;

[0015] **FIG. 2B** is a cross-sectional view through section line B-B of the catheter depicted in **FIG. 1**;

[0016] **FIG. 3** depicts a transition region between proximal and distal regions of the body of the catheter depicted in **FIG. 1**; and

[0017] **FIG. 4** depicts the transition region and distal region of an alternate preferred embodiment of a catheter according to the present invention.

#### DESCRIPTION OF SPECIFIC EMBODIMENTS

[0018] A catheter according to the present invention will comprise an elongate catheter body having proximal and distal ends and at least two regions, a proximal region and a distal region. The proximal region of the catheter body will have at least two lumens extending at least partly there-through. The distal region of the catheter body will have a single common lumen in communication with both of the lumens of the proximal region. Additionally, an inflatable angioplasty balloon will be disposed about the common lumen of the distal region of the catheter.

[0019] In use, a catheter according to the present invention will be advanced over a guidewire into a patient's vascular system. First, the guidewire will be advanced alone into the patient until the guidewire lies within a particular region of interest. This will typically be a region in which a blood vessel has been narrowed by a stenotic lesion. The distal end of the guidewire will be advanced into the region of stenosis with the proximal end of the guidewire remaining outside of the patient's body.

[0020] The proximal end of the guidewire may then be inserted into the distal end of the catheter body and fed through the common lumen of the distal region. When the proximal end of the guidewire reaches a transition region between the distal and proximal regions of the catheter body, the guidewire will be directed into a particular guidewire lumen of the proximal region.

[0021] Once the guidewire has been directed into the guidewire lumen, the catheter will be advanced into the patient's vascular system until the common lumen of the distal region lies within the region of interest. During advancement of the catheter into the blood vessel, the proximal end of the guidewire will exit the catheter body through a guidewire port located some distance proximal of the distal region (in either an "over-the-wire," configuration, or a "monorails" configuration). The proximal end of the guidewire may then be grasped and pulled back sufficiently to withdraw the distal end of the guidewire into the

guidewire lumen and clear of the common lumen of the distal region. An ultrasonic imaging transducer or other work element may then be advanced through another lumen of the proximal region and into the common lumen for imaging the region of interest.

[0022] Prior to inflation of the balloon, the imaging element will normally be withdrawn from the common lumen into its lumen in the proximal region. The guidewire will then be readvanced through the common lumen and into the blood vessel.

[0023] At present, it is highly advantageous for the guidewire to be in place in the common lumen when the balloon is inflated. When the balloon is inflated, blood flow through the blood vessel will be blocked by the balloon. An adverse ischemic condition may result and rapid removal of the catheter from the blood vessel may be required. If the guidewire is in position in the common lumen, rapid catheter removal will be made easier. Additionally, replacement of the catheter over the guidewire will be more convenient once the ischemic condition has abated.

[0024] After the initial balloon inflation, successive steps of imaging and dilation may be repeated as desired. Alternatively, some other form of interventional device, for example, a mechanical cutter or laser ablation device, may be advanced through the distal tip of the catheter body.

[0025] Thus, a catheter according to the present invention will allow for the convenient delivery of a balloon angioplasty device in combination with another interventional or imaging device to a region of interest within the patient. Because the catheter uses a single common distal lumen, it may be made with a reduced profile at its distal end. This will allow delivery of the balloon angioplasty imaging, or other interventional devices even within narrow, tortuous regions of the patient's vascular system. Furthermore, the various work elements are delivered through a common lumen lying within the balloon, thus minimizing the need to reposition the catheter body between treatment steps.

[0026] **FIG. 1** depicts a preferred embodiment of a catheter according to the present invention. The catheter has a catheter body **12**, which comprises proximal region **15**, distal region **18**, and transition region **20**. **FIG. 2A** is a cross-sectional view of the proximal region of catheter body **12** through section line A-A. In this embodiment, proximal region **15** has three lumens, work element lumen **23**, guidewire lumen **25**, and proximal balloon inflation lumen **27**. Other embodiments could have still more lumens to accommodate additional imaging or interventional devices, as described generally in U.S. Pat. No. 5,997,523, the full disclosure of which is incorporated herein by reference. Guidewire port **30** and balloon inflation port **32** (**FIG. 1**) place guidewire lumen **25** and proximal balloon inflation lumen **27** in communication with the exterior of the catheter near its proximal end.

[0027] In the embodiment depicted in **FIG. 1**, drive shaft **45** is reciprocatably disposed within work element lumen **23**. (For clarity, only a distal portion of drive shaft **45** is illustrated). At its proximal end, work element lumen **23** is in communication with expandable member **39**, which is connected in turn to proximal housing **35**. The proximal housing is adapted to connect a proximal end of drive shaft **45** to a drive motor (not shown) for rotating the drive shaft.

[0028] Expandable member 39 allows the drive shaft to be conveniently advanced and retracted within work element lumen 23 by moving proximal housing 35 with respect to the catheter body to lengthen or shorten expandable member 39 as desired. Proximal housing 35 is provided further with flush port 50, to allow for the flushing of trapped air bubbles from within work element lumen 23. The construction and use of proximal housing 35 in conjunction with a multi-lumen catheter is more fully described in U.S. Pat. No. 5,314,408, the full disclosure of which is incorporated herein by reference.

[0029] A cross-section through distal region 18 of catheter body 12 through section line B-B is depicted in FIG. 2B. As can be seen therein, distal region 18 has two concentric lumens. In the distal region, common lumen 60 is disposed within distal balloon inflation lumen 62.

[0030] Referring again to FIG. 1, balloon 65 is disposed about common lumen 60. The balloon is in communication with distal balloon inflation lumen 62 to provide for inflation of the balloon. Radiopaque band 68 is wrapped around the common lumen at a position within the balloon to allow for fluoroscopic imaging to assist in placing the balloon within the desired region of the blood vessel.

[0031] The length of common lumen 60 will generally be between 5 and 30 centimeters, with balloon 65 typically having a length in the range of 1.5-4.5 centimeters. The balloon crossing profile, the minimum width crossable by the balloon when deflated, will typically be in the range of 0.020-0.045 inches. The outside diameter of the balloon when inflated within a blood vessel will commonly be between 1.5 and 4.5 millimeters. The foregoing ranges are set forth solely for the purpose of illustrating typical device dimensions. The actual dimensions of a device constructed according to the principles of the present invention may obviously vary outside of the listed ranges without departing from those basic principles.

[0032] FIG. 3 depicts transition region 20 between the three parallel lumens of proximal region 15 and the two concentric lumens of distal region 18. Transition region 20 provides for communication between common lumen 60 of the distal region and both guidewire lumen 25 and work element lumen 23 of the proximal region. Also, distal balloon inflation lumen 62 is placed in communication with proximal balloon inflation lumen 27 through balloon inflation lumen connection 70, which is formed by cutting through the exterior of proximal region 15 to expose a portion of the proximal balloon inflation lumen and sealing the end of the balloon inflation lumen to close it off from common lumen 60. Thus, a continuous inflation path exists from balloon inflation port 32F through proximal and distal balloon inflation lumens 27 and 62, and into balloon 65. Injection of fluid into balloon inflation port 32 will thereby result in inflation of balloon 65.

[0033] It is contemplated that the catheter depicted in FIG. 1 will be used as follows. First, a conventional guidewire will be advanced into the patient's vascular system until it lies within the region of stenosis. Next, the guidewire will be inserted into distal tip 77 (FIG. 1) of the catheter and through common lumen 60 of distal region 18. The catheter will then be advanced into the patient's body over the guidewire until the guidewire reaches transition region 20. At this point, the guidewire will be directed into

guidewire lumen 25 and through the proximal region until it exits the catheter through guidewire port 30 as the catheter is advanced further into the patient's body. Eventually, the catheter will be advanced to a point where common lumen 60 and balloon 65 both lie within the region of interest.

[0034] The operator of the system can then grasp the guidewire at the end protruding from the guidewire port. The operator will pull the guidewire back a short distance into guidewire lumen 25 of proximal region 15 in order to clear common lumen 60 of distal region 18. A work element 75, which will typically be an ultrasonic imaging transducer, fixed to the distal end of drive shaft 45, may then be advanced through work element lumen 23 of the proximal region and into the common lumen of the distal region. Imaging of the region of interest may then take place.

[0035] Following imaging, work element 75 will be retracted into its lumen in the proximal region. The guidewire will be readvanced through the common lumen into the blood vessel. Balloon 65 may then be inflated to dilate the region of interest and thereby reduce the stenosis therein. Successive steps of imaging, guidewire replacement, and treatment may be repeated as desired until the stenosis has been satisfactorily reduced. If complications result due to restriction by the balloon of blood flow through the vessel, the catheter may be quickly and conveniently pulled back over the guidewire to restore blood flow through the vessel.

[0036] FIG. 1 depicts a catheter in which the common lumen is narrowed at a restriction 80 just proximal to the balloon. Distal of the restriction, the common lumen will be just large enough to allow passage of the guide wire. This allows the balloon crossing profile, the width of the catheter in the region of the balloon when not inflated, to be as small as possible. This is advantageous in that it allows the balloon to be advanced into narrow and tortuous regions of the blood vessel. Placing the restriction proximal to the balloon is disadvantageous, however, in that it may prevent entry of the work element into the common lumen within the balloon. Thus, some repositioning of the catheter body within the blood vessel, i.e., advancement of the catheter body a further into the blood vessel, may be necessary to allow for imaging of the treated region.

[0037] FIG. 4 depicts the distal region of an alternative preferred embodiment in which the common lumen is not restricted in the region proximal to the balloon. In this embodiment, the work element may travel through the common lumen into, through and beyond the balloon. This is advantageous in that it allows for imaging of the blood vessel throughout the region of the balloon without repositioning the catheter body.

[0038] As discussed above, it is desirable at present to have the guidewire in place within the common lumen during balloon inflation in case rapid withdrawal of the catheter over the guidewire becomes necessary. However, future developments in interventional devices and techniques may make this unnecessary. If this becomes the case, imaging will be possible from within the balloon even while the balloon is being inflated. Of course, an increased diameter common lumen within the balloon requires a slightly larger balloon crossing profile. Some ability to enter narrow regions must thereby be sacrificed in order to achieve a more flexible imaging capability.

[0039] The embodiment of **FIG. 4** depicts the common lumen having restriction **80** at some distance distal to balloon **65**. This restriction will prevent the accidental exit of the work element from the distal tip **77** of the catheter body while still allowing passage of the guidewire. This prevents injury to the blood vessel wall, which might result from accidental contact by the rotating work element. A catheter according to the present invention could also be made to carry an interventional work element such as a rotating cutter or a laser ablation device. In such a case, it would be necessary for the work element to advance beyond the distal tip **77** of the catheter body. In such a catheter system, restriction **80** would be omitted altogether to allow for unhindered passage of the work element.

[0040] Although the foregoing invention has been described in some detail by way of illustration and example for purposes of clarity of understanding, it will be obvious that certain changes and modifications may be practiced which will still fall within the scope of the appended claims.

1-12. (cancelled)

13. A catheter system comprising:

a catheter body having proximal and distal ends, and a proximal and a distal region, the proximal region having at least two lumens and the distal region having a common lumen connected to and in communication with both lumens of the proximal region;

an inflatable balloon disposed about at least a portion of the common lumen;

a drive shaft having proximal and distal regions, the drive shaft disposed within a lumen of the proximal region of the catheter body; and

a work element coupled to the distal region of the drive shaft, the work element positionable within the common lumen of the distal region of the catheter body.

14. The catheter system of claim 13, wherein the work element comprises an imaging device.

15. The catheter system of claim 14, wherein the imaging device comprises an ultrasonic transducer.

16. The catheter system of claim 13, wherein the work element is positionable within the balloon.

17. The catheter system of claim 13, wherein the work element is extendible to a position past the balloon and into a blood vessel.

18. The catheter system of claim 15, wherein the work element is positionable within the balloon.

19. The catheter system of claim 15, wherein the work element is extendible to a position past the balloon and into a blood vessel.

20. The catheter system of claim 19, wherein the work element comprises an imaging device.

21. The catheter system of claim 20, wherein the imaging device comprises an ultrasonic transducer.

22. The catheter system of claim 19, wherein the work element comprises an interventional device.

23. The catheter system of claim 14, further comprising:

an axially expandable member connected to the proximal end of the catheter body; and

a proximal housing connected to the proximal end of the drive shaft and the axially expandable member, whereby the work element may be advanced from a

position within a lumen of the proximal region into a position within the common lumen of the distal region by moving the proximal housing with respect to the catheter body.

24. The catheter system of claim 20, further comprising:

an axially expandable member connected to the proximal end of the catheter body; and

a proximal housing connected to the proximal end of the drive shaft and the axially expandable member, whereby the work element may be advanced from a position within a lumen of the proximal region into a position within the common lumen of the distal region by moving the proximal housing with respect to the catheter body.

25. The catheter system of claim 20, further comprising:

an axially expandable member connected to the proximal end of the catheter body; and

a proximal housing connected to the proximal end of the drive shaft and the axially expandable member, whereby the work element may be advanced from a position within a lumen of the proximal region into a position past the balloon by moving the proximal housing with respect to the catheter body.

26. The catheter system of claim 20, further comprising:

an axially expandable member connected to the proximal end of the catheter body; and

a proximal housing connected to the proximal end of the drive shaft and the axially expandable member, whereby the work element may be advanced from a position within a lumen of the proximal region into a position past the balloon and into a blood vessel by moving the proximal housing with respect to the catheter body.

27. The catheter system of claim 13, further comprising a balloon inflation means which includes a balloon inflation lumen disposed parallel to the two lumens of the proximal region.

28. The catheter system of claim 13, wherein the balloon inflation lumen lies within the catheter body at its proximal end and is disposed coaxially about the common lumen of the distal region of the catheter body.

29. A method for imaging and treating a region of a patient's blood vessel using a catheter system comprising a guidewire; an imaging device fixed to a distal portion of a drive shaft; a catheter body having a proximal region including at least two lumens, and a distal region including a common lumen connected to and in communication with both lumens of the proximal region; and an inflatable balloon disposed about at least a portion of the distal region; the method comprising the steps of:

advancing the guidewire in the blood vessel until a distal end portion of the guidewire lies within a region of interest, and a proximal end portion of the guidewire extends from the patient;

moving the proximal end portion of the guidewire into the common lumen of the distal region of the catheter body;

advancing the catheter body into the blood vessel until the balloon and the common lumen lie within the region of interest;

retracting the distal end portion of the guidewire out of the common lumen into a lumen of the proximal region of the catheter body;

advancing the imaging device and drive shaft through a lumen of the proximal region of the catheter body into the common lumen;

inflating the balloon to dilate the blood vessel; and

imaging the area of interest with the imaging device during the step of inflating the balloon.

**30.** The method of claim 29, wherein successive steps of imaging and balloon inflation are repeated as desired to reduce a stenosis at the region of interest to a desired extent.

**31.** The method of claim 29, wherein the balloon is an angioplasty balloon.

**32.** The method of claim 29, wherein the step of advancing the imaging device includes advancing the imaging device into the balloon.

**33.** The method of claim 29, wherein the step of advancing the imaging device includes advancing the imaging device past the balloon and into the blood vessel.

**34.** A method for treating a region of a patient's blood vessel using a catheter system comprising a guidewire; an interventional work element fixed to a distal region of a drive shaft; a catheter body having a proximal region including at least two lumens, and a distal region including a common lumen connected to and in communication with both lumens of the proximal region; and an angioplasty balloon disposed about at least a portion of the distal region; the method comprising the steps of:

advancing the guidewire into the blood vessel until a distal end portion of the guidewire lies within a region of interest and a proximal end portion of the guidewire extends from the patient;

moving the proximal end portion of the guidewire into the common lumen of the distal region of the catheter body;

advancing the catheter body into the blood vessel until the angioplasty balloon and the common lumen lie in the region of interest;

inflating the angioplasty balloon to dilate the blood vessel and reduce a stenosis at the region of interest;

retracting the distal end portion of the guidewire out of the common lumen into a lumen of the proximal region of the catheter body;

advancing the interventional work element through a lumen of the catheter body and through the common lumen into the blood vessel; and

treating the region of interest with the interventional device.

**35.** The method of claim 34, wherein the step of advancing the interventional work element includes advancing the interventional work element into the angioplasty balloon.

**36.** The method of claim 34, wherein the step of advancing the interventional work element includes advancing the interventional work element past the angioplasty balloon and into the blood vessel.

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