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(54) Title: A PHARMACEUTICAL COMPOSITION COMPRISING STABLE, AMORPHOUS HYBRID NANOPARTICLES OF AT LEAST ONE PROTEIN KINASE INHIBITOR AND AT LEAST ONE POLYMERIC STABILIZING AND MATRIX-FORMING COMPONENT

(57) Abstract: The present invention relates to the field of methods for providing pharmaceutical compositions comprising poorly water-soluble drugs. In particular the present invention relates to compositions comprising stable, amorphous hybrid nanoparticles, comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component, useful in pharmaceutical compositions and in therapy.



A pharmaceutical composition comprising stable, amorphous hybrid nanopartides of at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component.

Field of the invention

The present invention relates to the field of pharmaceutical compositions comprising poorly water-soluble drugs. In particular the present invention
5 relates to pharmaceutical compositions comprising stable, amorphous hybrid nanoparticles of protein kinase inhibitors (PKIs) and polymeric stabilizing and matrix-forming components. Furthermore, the present invention relates to a method of treating proliferative disorders in a patient in need thereof, comprising administering a therapeutically effective
10 amount of said compositions.

Background of the and invention

Components of cellular signal transduction pathways that regulate the growth and differentiation of normal cells can, when dysregulated, lead to
15 the development of cellular proliferative disorders and cancer. Mutations in cellular signaling proteins may cause such proteins to become expressed or activated at inappropriate levels or at inappropriate times during the cell cycle, which in turn may lead to uncontrolled cellular growth or changes in cell-cell attachment properties.

20

Many proliferative disorders, such as tumors and cancers, have been shown to involve overexpresion or upregulation of protein kinase activity. Protein kinases are kinase enzymes that modify proteins by chemically adding phosphate groups (phosphorylation). Phosphorylation usually
25 results in a functional change of the target protein by changing enzyme activity, cellular location, or association with other proteins. Protein kinases can be subdivided or characterised by the amino acids of the target protein whose phosphorylation they control: most kinases act on both serine and threonine, the tyrosine kinases act on tyrosine, and a number (dual-
30 specificity kinases) act on all three. There are also protein kinases that phosphorylate other amino acids, including histidine kinases that phosphorylate histidine residues. The human genome contains about 500

protein kinase genes and up to 30% of all human proteins may be modified by protein kinases. Kinases are known to regulate the majority of cellular pathways, especially those involved in signal transduction. Dysregulation of protein kinases by mutation, gene rearrangement, gene amplification, and overexpression of both receptor and ligand has been implicated in the development and progression of human cancers. Protein kinase inhibiting compounds or protein kinase inhibitors (PKIs) are therefore useful for treating diseases caused by or exacerbated by overexpression or upregulation of protein kinases. For example, tyrosine kinase inhibitors (TKIs also known as tyrphostins) have been shown be effective anti-tumor agents and anti-leukemic agents (Lowery A et. al., Front Biosci. 2011 Jun 1;17:1996-2007).

A major objective of formulation chemistry is to improve drug efficiency and safety, by e.g. improving bioavailability and stability as well as convenience to the patient. Bioavailability means the rate and extent to which an active substance or therapeutic is absorbed from a pharmaceutical form and becomes available at the site of action. The most common and preferred method of delivery due to convenience, ease of ingestion, and high patient compliance to treatment is the oral route of drug delivery. However, for certain drugs, drug absorption from the gastrointestinal tract is limited by poor aqueous solubility and/or poor membrane permeability of the drug molecules.

PKIs are generally weak bases that dissolve only slightly at low pH (e.g. 100-1000 mg/L) and are practically insoluble at neutral pH (e.g. 0.1-10 mg/L). Therefore, enhancing the solubility and dissolution rate of PKI-based drugs is important for improving the bioavailability and efficacy of most of these drugs. Typical PKIs exhibit non-polypeptide structure and have relatively low molecular weights, such as ≤ 10000 dalton or ≤ 5000 dalton.

Several methods to improve the dissolution characteristics of poorly water soluble drugs have been reported, including micronisation, formation of salts or solvates, complexes and microspheres. Additionally, attempts have been made to improve bioavailability provided by solid dosage forms
5 by forming particles comprising the drug or by mixing the poorly water soluble drug with hydrophilic excipients. Traditionally, however, these methods carry inherent limitations concerning physical stabilities of the particles on storage, problems with grinding or difficulty of removal of the frequently toxic solvent. Furthermore, it is important that the drug released
10 from the solid phase does not precipitate in the gastrointestinal tract, or precipitates as little as possible, but remains water-soluble in the aqueous fluids of the gastrointestinal tract, since such precipitation results in low bioavailability (see e.g. Hervé J. et al. Pharm Dev Technol. 2011 Jun; 16(3):278-86).

15 pH-dependent solubility is a well-known issue for many oral formulations of poorly water-soluble substances, such as PKIs, since most of the absorption of the drug occurs in the small and large intestine, where pH is close to neutral. There is thus a continuing need to develop and improve
20 the dissolution characteristics of oral solid dosage forms of PKI-based drugs. (Budha NR, Frymoyer A, Smelick GS, Jin JY, Yago MR, Dresser MJ, Holden SN, Benet LZ, Ware JA. Clin Pharmacol Ther. 2012 Aug;92(2):203-13). Therefore, methods for improving dissolution of PKI-based drugs, as well as of other poorly water-soluble drugs, at neutral
25 (intestinal) pH are highly desirable.

US20090203709 discloses a pharmaceutical dosage form comprising a solid dispersion product of at least one tyrosine kinase inhibitor, at least one pharmaceutically acceptable polymer and at least one
30 pharmaceutically acceptable solubilizer. Further the reference discloses methods for preparing the above-mentioned pharmaceutical dosage form, comprising preparing the homogenous melt of at least one tyrosine kinase

inhibitor, at least one pharmaceutically acceptable polymer and at least one pharmaceutically acceptable solubilizer, and allow the melt to solidify to obtain a solid dispersion product.

EP2105130 discloses pharmaceutical formulations comprising a solid dispersion or solid solution, containing a polymer and an active agent in amorphous form. Further, the formulation comprises an external polymer to stabilize the solution, such that the % by weight of the external polymer is less than 20% of the total weight of the pharmaceutical formulation. Additionally, the reference discloses a hot melt extrusion method for production of the above-mentioned formulation.

Any discussion of the prior art throughout the specification should in no way be considered as an admission that such prior art is widely known or forms part of common general knowledge in the field.

It is an object of the present invention to overcome or ameliorate at least one of the disadvantages of the prior art, or to provide a useful alternative.

Summary of the invention

The present invention relates pharmaceutical compositions comprising stable, amorphous hybrid nanoparticles, comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component. Optionally, one or more solubilizers may be added to the particles, present separately from the particles, or within the particles.

According to a first aspect, the present invention provides a pharmaceutical composition comprising stable, amorphous solid dispersion particles of dasatinib and at least one polymeric stabilizing and matrix-forming component; which composition optionally further comprises at least one pharmaceutically acceptable solubilizer; wherein said dasatinib is present in an amount of from about 10% by weight to about 70% by weight of the amorphous particles; wherein the particles are obtained by mixing i) a pressurized solution comprised of dasatinib and a solvent and ii) a pressurized antisolvent, and wherein said at least one polymeric stabilizing and matrix-forming component is provided in either one or both of the pressurized solution or the pressurized antisolvent.

According to a second aspect, the present invention provides use of a composition according to the first aspect, in the manufacture of a medicament.

According to a third aspect, the present invention provides use of a composition according to the first aspect, in the manufacture of a medicament for the treatment of proliferative disorders.

According to a fourth aspect, the present invention provides use of a composition according to the first aspect for therapy.

According to a fifth aspect, the present invention provides use of a composition according to the first aspect, for the treatment of proliferative disorders.

According to a sixth aspect, the present invention provides a method of providing therapy comprising administering to a patient in need thereof a composition according to the first aspect.

According to a seventh aspect, the present invention provides a method of treating proliferative disorders comprising administering to a patient in need thereof a composition according to the first aspect.

Unless the context clearly requires otherwise, throughout the description and the claims, the words "comprise", "comprising", and the like are to be construed in an inclusive sense as opposed to an exclusive or exhaustive sense; that is to say, in the sense of "including, but not limited to".

Brief description of the drawings

Figure 1 provides a graph showing the apparent solubility for nilotinib in representative compositions of the invention. Further experimentation with both nilotinib base and nilotinib HCl is found in Example 1 . The details of the particles are described in Example 1 , Table 1 , for experiment 3, 30 and 37, respectively. Briefly, experiment 30 represents stable, amorphous hybrid nanoparticles comprising nilotinib HCl and HPMCP HP55 and wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate- polyethylene glycol copolymer is present separately from the hybrid nanoparticles. Experiment 3 represents raw, crystalline nilotinib HCl and experiment 37 represents hybrid nanoparticles of nilotinib HCl, HPMCP HP55 and the solubilizer polyvinyl caprolactam-polyvinyl acetate- polyethylene glycol copolymer, present within the hybrid nanoparticles.

The experiments illustrated in the graphs were carried out at pH 6.5, in FaSSIF.

Figure 2 provides a graph showing the apparent solubility for erlotinib in representative compositions of the invention. Further experimentation with erlotinib is found in Example 2. The details of the stable, amorphous hybrid nanoparticles are described in Example 2, Table 7, for experiment 58, 65 and 67, respectively. Briefly, experiment 65 represents stable, amorphous hybrid nanoparticles with erlotinib HCl and HPMC-AS, wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. Experiment 58 represents raw, crystalline erlotinib HCl and experiment 67 represents stable, amorphous hybrid nanoparticles of erlotinib HCl, HPMC-AS and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer present within the hybrid nanoparticles. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

Figure 3 provides a graph showing the apparent solubility for pazopanib in representative compositions of the invention. Further experimentation with pazopanib is found in Example 3. The details of the stable, amorphous hybrid nanoparticles are described in Example 3, Table 13, for experiment 84, 91 and 93, respectively. Briefly, experiment 91 represents stable, amorphous hybrid nanoparticles comprising pazopanib and PVP 90K and wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles, experiment 93 represents hybrid nanoparticles comprising pazopanib, PVP 90K and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer, present within the stable, amorphous hybrid nanoparticles. Experiment 84 represents raw, crystalline pazopanib. The experiments illustrated in the graphs were carried out at pH 6.5, in FaSSIF.

Figure 4 provides a graph showing the apparent solubility for lapatinib in representative compositions of the invention. Further experimentation with both lapatinib base and lapatinib ditosylate salt is found in Example 4. The details of the stable, amorphous hybrid nanoparticles are described in Example 4, Table 19, for experiment 110, 122 and 126, respectively. Briefly, experiment 122 represents stable, amorphous hybrid nanoparticles comprising lapatinib base and HPC EF, wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. Experiment 110 represents raw, lapatinib base and experiment 126 represents stable, amorphous hybrid nanoparticles of lapatinib base, HPC LF and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer present within the hybrid nanoparticles. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

Figure 5 provides a graph showing the apparent solubility for nilotinib in representative compositions of the invention. The details of the stable, amorphous hybrid nanoparticles are described in Example 5, Table 21, for experiment 127, 128 and 129, respectively. Briefly, experiment 129 represents a physical mixture of raw, crystalline nilotinib HCl, HPMCP HP55 and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer. Experiment 128 represents stable, amorphous hybrid nanoparticles comprising nilotinib HCl and HPMCP HP55, wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. Experiment 127 represents stable, amorphous hybrid nanoparticles of nilotinib HCl and HPMCP HP55. The experiments illustrated in the graphs were carried out at pH 1.4 in SGF.

Figure 6 provides a graph showing the apparent solubility for gefitinib in representative compositions of the invention. Further experimentation with

gefitinib is found in Example 6. The details of the compositions are described in Example 6, Table 22, for experiment 131, 133, 135 and 137, respectively. Briefly, experiment 131 represents raw, crystalline gefitinib. Experiment 133 represents a mixture of raw, crystalline gefitinib, HPMCP HP55 and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer. Experiment 135 represents stable, amorphous hybrid nanoparticles of gefitinib and HPMCP HP55. Experiment 137 represents stable, amorphous hybrid nanoparticles of gefitinib and HPMCP HP55 wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

Figure 7 provides a graph showing the apparent solubility for dasatinib in representative compositions of the invention. The details of the stable, amorphous hybrid nanoparticles are described in Example 7, Table 24, for experiments 138-141. Briefly, experiment 138 represents raw, crystalline dasatinib. Experiment 139 represents a mixture of raw, crystalline dasatinib, Kollidon VA64 and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer. Experiment 140 represents hybrid nanoparticles of dasatinib and Kollidon VA64. Experiment 141 represents stable, amorphous hybrid nanoparticles of dasatinib and Kollidon VA64 wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

Figure 8 provides a graph showing the apparent solubility for sorafenib in representative compositions of the invention. The details of the stable, amorphous hybrid nanoparticles are described in Example 8, Table 26, for experiments 142-145. Briefly, experiment 142 represents raw, crystalline sorafenib tosylate. Experiment 143 represents a mixture of raw, crystalline

sorafenib tosylate, HPMCP HP55 and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer. Experiment 144 represents stable, amorphous hybrid nanoparticles of sorafenib tosylate and HPMCP HP55. Experiment 145 represents hybrid nanoparticles of sorafenib tosylate and HPMCP HP55 wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

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Figure 9 provides a graph showing the apparent solubility for crizotinib in representative compositions of the invention. Further experimentation with crizotinib is found in Example 10. The details of the compositions are described in Example 10, Table 30, for experiment 150, 152, 153 and 156, respectively. Briefly, experiment 150 represents raw, crystalline crizotinib. Experiment 152 represents a mixture of raw, crystalline crizotinib, PVP 30K and the solubilizer Cremophor RH40. Experiment 153 represents stable, amorphous hybrid nanoparticles of crizotinib and PVP 30K. Experiment 156 represents stable, amorphous hybrid nanoparticles of crizotinib and PVP 30K wherein the solubilizer Cremophor RH40 is present separately from the stable, amorphous hybrid nanoparticles. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

Figure 10 provides a graph showing the apparent solubility for axitinib in representative compositions of the invention. Further experimentation with axitinib is found in Example 11. The details of the compositions are described in Example 11, Table 32, for experiment 157, 158, 160 and 162, respectively. Briefly, experiment 157 represents raw, crystalline axitinib. Experiment 158 represents a mixture of raw, crystalline axitinib, Kollidon VA64 and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer. Experiment 160 represents stable, amorphous hybrid nanoparticles of axitinib and Kollidon VA64. Experiment

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162 represents stable, amorphous hybrid nanoparticles of axitinib and Kollidon VA64 wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. The experiments illustrated in the
5 graphs were carried out at pH 6.5 in FaSSIF.

Figure 11 provides a graph showing the apparent solubility for vemurafenib in representative compositions of the invention. Further experimentation with vemurafenib is found in Example 12. The details of the compositions
10 are described in Example 12, Table 34, for experiment 164, 166, 168 and 170, respectively. Briefly, experiment 164 represents raw, crystalline vemurafenib. Experiment 166 represents a mixture of raw, crystalline vemurafenib, CAP and the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer. Experiment 168 represents stable,
15 amorphous hybrid nanoparticles of vemurafenib and CAP. Experiment 170 represents stable, amorphous hybrid nanoparticles of vemurafenib and CAP wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer is present separately from the stable, amorphous hybrid nanoparticles. The experiments illustrated in the graphs
20 were carried out at pH 6.5 in FaSSIF.

Figure 12 provides a graph showing the dissolution rate for nilotinib base in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.1, and Table 36 for
25 experiments 500 and 501. Briefly, experiment 500 represents raw, nilotinib HCl. Experiment 501 represents stable, amorphous hybrid nanoparticles of nilotinib base and HPMCP HP55. The experiments illustrated in the graphs were carried out at pH 6.5 in FaSSIF.

30 Figure 13 provides a graph showing the dissolution rate for erlotinib in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.2, Table 37 for

experiments 510 and 511. Briefly, experiment 510 represents raw, erlotinib HCl. Experiment 511 represents stable, amorphous hybrid nanoparticles of erlotinib HCl and HPMC AS.

- 5 Figure 14 provides a graph showing the dissolution rate for pazopanib in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.3, Table 38 for experiments 520 and 521. Briefly, experiment 520 represents raw, pazopanib HCl. Experiment 521 represents stable, amorphous hybrid
10 nanoparticles of pazopanib HCl and PVP90K.

- Figure 15 provides a graph showing the dissolution rate for lapatinib in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.4, Table 39 for
15 experiments 530 and 531. Briefly, experiment 530 represents raw, lapatinib ditosylate. Experiment 531 represents stable, amorphous hybrid nanoparticles of lapatinib base and HPC If.

- Figure 16 provides a graph showing the dissolution rate for gefitinib in
20 representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.5., Table 40 for experiments 540 and 541. Briefly, experiment 540 represents raw, gefitinib. Experiment 541 represents stable, amorphous hybrid nanoparticles of gefitinib and HPMCP HP55.

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- Figure 17 provides a graph showing the dissolution rate for dasatinib in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.6., Table 41 for experiments 550 and 551. Briefly, experiment 550 represents raw,
30 dasatinib. Experiment 551 represents stable, amorphous hybrid nanoparticles of dasatinib and Kollidon VA64.

Figure 18 provides a graph showing the dissolution rate for sorafenib in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.7., Table 42 for experiments 560 and 561. Briefly, experiment 560 represents raw,
5 sorafenib tosylate. Experiment 561 represents stable, amorphous hybrid nanoparticles of sorafenib tosylate and HPMCP HP55.

Figure 19 provides a graph showing the dissolution rate for crizotinib in representative compositions of the invention, measured under sink
10 conditions. Details are found in Examples 13 and 13.8., Table 43 for experiments 570 and 571. Briefly, experiment 570 represents raw, crizotinib. Experiment 571 represents stable, amorphous hybrid nanoparticles of crizotinib and PVP 30K.

15 Figure 20 provides a graph showing the dissolution rate for axitinib in representative compositions of the invention, measured under sink conditions. Details are found in Examples 13 and 13.9., Table 44 for experiments 580, 581 and 582. Briefly, experiment 580 represents raw, axitinib. Experiment 581 represents hybrid nanoparticles of axitinib and
20 Kollidon VA64 and experiment 582 represents stable, amorphous hybrid nanoparticles of axitinib and HPMC AS.

Figure 21 provides a graph showing the dissolution rate for vemurafenib in representative compositions of the invention, measured under sink
25 conditions. Details are found in Examples 13 and 13.10., Table 45 for experiments 590, 591 and 592. Briefly, experiment 590 represents raw, vemurafenib. Experiment 591 represents hybrid nanoparticles of vemurafenib and Kollidon VA64 and experiment 592 represents stable, amorphous hybrid nanoparticles of vemurafenib and CAP.

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Figure 22 provides graphs showing *in vivo* measurement of plasma levels after oral administration to beagle dogs of representative compositions

comprising stable, amorphous hybrid nanoparticles of nilotinib base and the polymeric stabilizing and matrix-forming components PVAP and HPMCP HP55, respectively (I/P), denoted PVAP and HP55, as well as wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-
5 polyethylene glycol copolymer was added (I/P+S), denoted HP55s and PVAPs, respectively. The experiments were carried out in beagle dogs pre-treated to have neutral stomach content. The stable, amorphous hybrid nanoparticles are further described in experiments 146 and 147 (Example 9) and details of the *in vivo* experiments are set out in Example 14. The
10 experiments used a marketed formulation comprising nilotinib HCl ("Tasigna") as reference.

Figure 23 provides graphs showing *in vivo* measurement of plasma levels after oral administration to beagle dogs of representative compositions
15 comprising stable, amorphous hybrid nanoparticles of nilotinib base and the polymeric stabilizing and matrix-forming components PVAP and HPMCP HP55, respectively (I/P), denoted PVAP and HP55, as well as wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-
polyethylene glycol copolymer was added (I/P+S) denoted PVAPs and
20 HP55s, respectively. The experiments were carried out in beagle dogs pre-treated to have acidic stomach content. The stable, amorphous hybrid nanoparticles are further described in experiments 146 and 147 (Example 9) and details of the *in vivo* experiments are set out in Example 14. The experiments used a marketed formulation comprising nilotinib HCl
25 ("Tasigna") as reference.

Figure 24 provides graphs showing *in vivo* measurement of plasma levels after oral administration to beagle dogs of representative compositions
30 comprising stable, amorphous hybrid nanoparticles of nilotinib base and the polymeric stabilizing and matrix-forming components PVAP and HPMCP HP55, respectively (I/P), denoted PVAP and HP55, as well as wherein the solubilizer polyvinyl caprolactam-polyvinyl acetate-

polyethylene glycol copolymer was added after hybrid nanoparticle formation (I/P+S), denoted PVAPs and HP55s, respectively. The experiments were carried out in beagle dogs pre-treated to have acidic or neutral stomach content. The stable, amorphous hybrid nanoparticles are
5 further described in experiments 146 and 147 (Example 9) and details of the *in vivo* experiments are set out in Example 14.

Figure 25 provides graphs showing *in vivo* measurement of plasma levels after oral administration to beagle dogs of representative compositions
10 comprising stable, amorphous hybrid nanoparticles of nilotinib base and the polymeric stabilizing and matrix-forming components PVAP and HPMCP HP55, denoted PVAP and HP55, respectively (I/P). The experiments were carried out in beagle dogs pre-treated to have acidic or neutral stomach content. The stable, amorphous hybrid nanoparticles are
15 further described in experiments 146 and 147 (Example 9) and details of the *in vivo* experiments are set out in Example 14.

Figure 26 provides a graph showing the apparent solubility of representative compositions before and after 11 months of storage at room
20 temperature. The experiment provides stable, amorphous hybrid nanoparticles comprising nilotinib base, HPMCP HP55 and the addition of the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (I/P+S) as Exp 171 & Exp 172 with further details set out in Example 15.

25

Figure 27 provides overlaid X-ray powder diffraction (XRPD) patterns of stable hybrid nanoparticles at 40% drug load, I/P nilotinib base/HPMCP HP55. Initial (top) and after 12 months storage at ambient temperature (bottom). The XRPD patterns are offset in order improve the visual
30 comparison. Further details are set out in Example 15.

Detailed description of the invention

All patents, patent applications, and publications cited herein are hereby incorporated by reference in their entirety.

5 As used herein, the phrase “hybrid nanoparticles” refers to a group of particles, typically in the average size range of from 1 to 1000 nm, composed of at least two components, one of which is the PKI and the other a polymeric stabilizing and matrix-forming component. The particles can be either crystalline or amorphous, or a mixture thereof. Typically, in
10 the sense of the present disclosure, the particles are “amorphous”, or “essentially amorphous”. This means that almost all, if not all, content of the particles comprise amorphous protein kinase inhibitor and polymeric stabilizing and matrix-forming component. The level or degree of amorphicity is at least 60%, such as 70%, such as 80% or 85%, preferably
15 at least 90% and more preferably >95%, wherein 100% represents that all material is amorphous in the particles.

Quantification of crystalline PKI or absence of crystalline PKI may be measured by X-ray powder diffraction methods as described in Saleki-
20 Gerhardt A et al. Int J Pharm. 1994;101:237–247) or by water vapor sorption as described in Dash AK et al. J Pharm Sci. 2002 Apr;91(4):983-90.

The term “solid dispersion particles” relates to “hybrid nanoparticles” as
25 defined above, however, solid dispersion particles are typically larger or much larger in size (typically μm -mm, as described in Wu K. et al. J Pharm Sci. 2009 Jul;98(7):2422-3). The smaller size of hybrid nanoparticles contributes to further stabilizing the PKI against crystallization. Typically, hybrid nanoparticles is in the average size range of from 1 to 1000 nm,
30 such as below 500 nm, preferably below 250 nm.

The phrase “stable” refers to the level of stability of produced particles by the methods of the present invention and may be measured as the capability of the hybrid nanoparticles to remain in their physical state for 6-12 months storage at ambient temperature (e.g. 18-25°C). The level of stability may be measured by AUC measurements of dissolution rate over for instance 80 minutes of the particles, after such storage.

By the phrase “protein kinase inhibitor” or “PKI” is meant a type of enzyme inhibitor that specifically blocks the action of one or more protein kinases. PKIs include, but are not limited, to protein kinase inhibitors and tyrosine kinase inhibitors, such as axitinib, afatinib, bosutinib, crizotinib, cediranib, dasatinib, erlotinib, fostamatinib, gefitinib, imatinib, lapatinib, lenvatinib, lestaurtinib, motesanib, mubritinib, nilotinib, pazopanib, pegaptanib, ruxolitinib, sorafenib, semaxanib, sunitinib, tandunitib, tipifamib, vandetanib and vemurafenib; or salts or hydrates or solvates thereof, or combinations thereof.

By the phrase “polymeric stabilizing and matrix-forming component” is meant the component present in the hybrid nanoparticles together with the PKI. Typically, said polymeric stabilizing and matrix-forming component exhibits a polymeric structure, such as, but not limited to, methyl cellulose, hydroxyethyl cellulose, hydroxypropyl cellulose (e.g. HPC ef, HPC lf and HPC jf), hydroxypropyl methylcellulose (e.g. Methocel E3 and E15 and Pharmacoat), hydroxypropyl methylcellulose acetate succinate (HPMC AS), hydroxypropyl methylcellulose phthalate (e.g. HPMCP-HP55), polyvinylpyrrolidone (e.g. PVP 30K and PVP 90K), polyvinyl acetate phthalate (PVAP), copolyvidone (e.g. Kollidon VA 64), crospovidon (e.g. Kollidon CL), methacrylic acid and ethylacrylate copolymer (e.g. Kollicoat ME), methacrylate acid and methyl methacrylate copolymer (e.g. Eudragit L100), polyethylene glycol (PEG), DL lactide/glycolide copolymer, poly DL-lactide, cellulose acetate phthalate (CAP), aminoalkyl methacrylate copolymers (e.g. Eudragit RL100, RL PO or RS PO), carbomer

homopolymer Type A (e.g. Carbopol 971P), carbomer homopolymer Type B (e.g. Carbopol 974P) and Poloxamers (e.g. Pluronic, Kolliphor).

5 The term “polymer” or “polymeric” is here used to mean a compound that is made of monomers connected together to form a larger molecule. A polymer generally consists of 20 or more monomers connected together, however less than 20 monomers connected together are here also referred to as polymers.

10 The term “solubilizer” is here used to mean a compound that increases the solubility of a substance, such as, but not limited to, polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus), d- α -tocopherol acid polyethylene glycol 1000 succinate (TPGS), PEG-40 hydrogenated castor oil (Cremophor RH40), PEG-35 castor oil (Cremophor EL), PEG-40
15 stearate (MYRJ 540), hard fat (e.g. Gelucire 33/01), polyoxylglycerides (e.g. Gelucire 44/14), stearyl polyoxylglycerides (e.g. Gelucire 50/13), PEG-8 caprylic/capric glycerides (e.g. Labrasol) and Poloxamers (e.g. Pluronic, Kolliphor).

20 As used herein, the phrase “primary particles” refers to the smallest particulate entities formed during the precipitation process. The boundaries of the particles are analyzed by SEM microscopy. Depending on process parameters, the primary particles may build together a more or less dense and porous network forming larger, agglomerated or bridging particles.
25 Parameters affecting the agglomeration are e.g. temperature that may modify the softness of the primary particles; ratio solvent/antisolvent affecting precipitation time, concentration of the PKI solution; and the nature of the polymeric stabilizing and matrix-forming agent(s). The average size of the primary particles is typically between 1 to 1000 nm,
30 preferably below 500 nm, more preferably below 250 nm.

As used herein, the phrases “supercritical” and “supercritical fluid” refer to that a chemical substance that is set to both a temperature higher or equal than its critical temperature (T_c) and a pressure higher or equal than its critical pressure (P_c).

5

As used herein, the phrases “subcritical” and “subcritical fluid” refer here to that one of critical temperature (T_c) or critical pressure (P_c) is set to a temperature or pressure higher than its critical temperature (T_c) or critical pressure (P_c), respectively, and the other of critical temperature (T_c) or critical pressure (P_c) is set to a temperature or pressure lower than its critical temperature (T_c) or critical pressure (P_c), respectively.

10

By the phrase “area under the curve (AUC)” is meant the area under the concentration-time curve, where the x-axis represents time and the y-axis represents solubilized drug concentration.

15

By the phrase “apparent solubility” is meant the concentration of material at apparent equilibrium. See further in the Examples section.

20 The term “supersaturation” is here used to mean that a solution contains more of the dissolved substance than could be dissolved by the solvent or media under normal circumstances.

As used herein, the term “Soluplus” or “soluplus” refers to polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer.

25

As used herein, the term “TPGS” refers to d- α -tocopherol acid polyethylene glycol 1000 succinate.

30 As used herein, the term “Chremophor RH40” refers to PEG-40 hydrogenated castor oil.

As used herein, the term "PVAP" refers to polyvinyl acetate phthalate.

As used herein, the term "PVP 90K" refers to polyvinylpyrrolidone K-90.

5 As used herein, the term "PVP 30K" refers to polyvinylpyrrolidone K-30.

As used herein, the term "HPMC-AS" refers to hydroxypropyl methylcellulose acetate succinate.

10 As used herein, the term "HPMCP HP55" refers to hydroxypropyl methyl cellulose phthalate.

As used herein, the term "HPC" refers to hydroxypropyl cellulose, such as HPC EF and HPC LF.

15

As used herein, the term "Kollidon VA64" refers to copolyvidone.

As used herein, the term "CAP" refers to cellulose acetate phthalate.

20 The dissolution mediums used for purposes of testing hybrid nanoparticles of the present invention, includes Fasted State Stimulated Intestinal Fluid, referred to as FaSSIF, Fed State Stimulated Intestinal Fluid, referred to as FeSSIF, and Simulated Gastric Fluid, referred to as SGF. FaSSIF media is tailored to represent a fasting state and has a pH of about 6.5 as well as
25 particular osmolaric properties. FeSSIF media is tailored to represent a fed state and has a pH of about 5 as well as specific osmolaric properties. SGF is tailored to represent gastric fluid and has a pH of about 1.4 as well as particular osmolaric properties. FaSSIF, FeSSIF and SGF media are generally used in *in vitro* models for dissolution of poorly water-soluble
30 drugs. The choice of medium will be dependent of the where in the intestinal tract and under what conditions (fasted or fed) particles are desired to dissolve and be taken up. Further details regarding these fluids

are described in e.g. Hervé J. et al. Pharm Dev Technol. 2011 Jun; 16(3):278-86 and Jantratid, E., and Dressman, J. Dissolut. Technol. 2009 8, 21-25.

- 5 By the phrase “amorphous form” is meant non-crystalline solid form. The ease of dissolution may at least in part be attributed to the amount of energy required for dissolution of the components from a crystalline or amorphous solid phase. Amorphous particles require less energy for dissolution as compared to crystalline particles of the same compound.

10

The inventive compositions comprise particles with a PKI or a combination of two or more PKIs. However, the particles may comprise a combination of one or more PKIs and at least one further active ingredient, such as one or more drugs. Various kinds of PKIs can be effectively utilized.

15

The term PKIs (protein kinase inhibitors) as used herein, is intended to include also the hydrates, solvates (alcoholates), pharmaceutically acceptable acid salts, base salts or co-crystals of such protein kinase inhibiting compounds.

20

As used herein, the term water-insoluble or poorly water soluble (or hydrophobic) compounds, refers to compounds whose solubility in water at 25° C is less than 1 g/100 ml, especially less than 0.1 g/100 ml in pure water at neutral pH.

25

The stable, amorphous hybrid nanoparticles comprised in the compositions of the present invention are typically in the form of particles as described elsewhere in this specification. There are a number of different methods for the formation of larger particles, e.g. granulation, melt extrusion, spray
30 drying, precipitation etc. all of which typically encompass starting with formation of a mixture between the Active Pharmaceutical Ingredient (API) and the polymeric stabilizing and matrix-forming component. The particles

comprised in the compositions of the present invention are produced with continuous processes for generating hybrid nanoparticles. Continuous processes in this context means that particle formation is continuously ongoing while at the same time continuously withdrawing/collecting/
5 retaining hybrid nanoparticles from the mixture after their formation. In the preferred methods, i.e. precipitation methods, this means that a fluid which is a solution of the PKI, preferably in the form of a fluid stream, is mixed with an antisolvent fluid, preferably in the form of an antisolvent fluid stream. The polymeric stabilizing and matrix-forming component may be
10 present in either one or both of the two fluids depending on its solubility characteristics. The mixing of the two fluids is taking place in a mixing function, e.g. a mixing chamber. In the case the process is continuous, i.e. the two fluids are fluid streams, the mixing function typically is associated with a particle formation and separation function wherein the mixed fluid
15 stream may pass through while retaining the hybrid nanoparticles. Agents modifying the particle characteristics without being incorporated into the particles may be added to either one or both of the two fluids before the mixing step. The fluids typically are conventional liquids or supercritical fluids, where supercritical fluids also include subcritical fluids (i.e. fluids for
20 which only one of pressure and temperature is above its supercritical value). Typical combinations are, a) conventional (i.e., non-supercritical) liquids for both the API solution and the antisolvent, b) supercritical solution of the API combined with conventional liquid for the antisolvent, c) conventional liquid for the API solution combined with supercritical fluid for the antisolvent, and d) supercritical fluids for both of the two fluids. In
25 certain variants the antisolvent may be omitted. A fluid stream, preferably supercritical, containing both the API and the polymeric stabilizing and matrix-forming component is then allowed to expand into the particle formation function. It is preferred that at least one of the fluids is in a
30 supercritical state in the precipitation methods described above. These kinds of precipitation methods are discussed in WO 2005061090 (Censdelivery AB), WO 2009072950 (XSpray Microparticles AB), WO

2009072953 (XSpray Microparticles AB), WO 2011159218 (XSpray Microparticles AB) and references cited in these publications.

The term "solution" encompasses that the solute is either a true solute or
5 minute particles of colloidal dimensions (typically 1-1000 nm) and less than the particles to be produced.

A preferred particle formation system is the "Right Size system" developed by XSpray Microparticles AB, Sweden. A detailed description of the
10 technology can be found in the WO-publications given in the preceding paragraph. An important characteristic of the system is that the two fluid streams should merge within a nozzle at an angle in the interval 45°-135°, with preference for about 90° and sprayed into a particle formation/separation function. In principle the system allows for producing
15 particles of predetermined size and/or morphology. Here the Right Size system and apparatus will be described using the non-limiting example of a PKI as the drug and CO₂ as a supercritical fluid antisolvent.

The system consists of one pumping set-up for the PKI dissolved in a
20 liquid solvent, referred to as the API solution, and one pumping set-up for an antisolvent, for example CO₂, however also other antisolvents may be used when suitable. Each pumping set-up includes instruments such as a flow meter and a pressure meter that are used to control the process conditions. These two pumping set-ups are fluidically connected at a spray
25 nozzle.

A stream of liquid API solution is mixed with a stream of CO₂ under flow conditions within the spray nozzle. The polymeric stabilizing and matrix-forming component is present in either the API solution or in the stream of
30 CO₂. These streams are sprayed at the outlet of the nozzle into a precipitation vessel under controlled conditions (typically pressure and temperature). CO₂ acts as an antisolvent and makes the API to precipitate

together with the polymeric stabilizing and matrix-forming component into fine particles. Particles are retained in the vessel by a filtering set-up. A back pressure regulator is typically used to control the pressure inside the precipitation vessel.

5

For preparing hybrid nanoparticles of certain drugs, for example but not limited to pazopanib and erlotinib, it may be advantageous to have an extra pumping set-up for injecting an additional solvent, referred to as a modifier, into the CO₂. Here a pumping set-up control is set up for the
10 modifier and the modifier is mixed with the CO₂ in a mixer before entering the nozzle.

When using the system, the system operator typically starts by equilibrating the system by pumping CO₂, an "PKI like solution" (a solution
15 similar in composition to the PKI solution but containing no PKI and no excipient) and the modifier (if used) through the system until flow rates, pressure and temperature have reached a desired steady state. Critical parameters for setting up the system are PKI solution composition, PKI solution flow rate, CO₂ flow rate, CO₂ pressure and temperature, nature of
20 the modifier and modifier flow rate, if such is used.

Next, the "PKI like solution" is exchanged for the PKI solution and particles are produced and retained downstream of the mixing, e.g. downstream of the outlet of the nozzle. Afterwards, the system is typically
25 cleaned by pumping the "PKI like solution" through the system. The particles are dried by flushing CO₂ through the retained particles in order to extract any remaining solvent. The precipitation vessel is then depressurized and the particles can be collected.

30 The solution/solvent and the antisolvent are typically miscible with each other. The pressure and temperature in the particle formation function,

and/or upstream of this function, such as in the mixing function, provide supercritical or subcritical conditions in relation to the antisolvent.

The concentration of the PKI in the solution is typically below its saturation
5 concentration, such as $\leq 50\%$, such as $\leq 60\%$, such as $\leq 75\%$, such as
 $\leq 85\%$ or such as $\leq 95\%$ of the saturation concentration. Suitable
concentrations are typically found in the interval $\leq 20\%$, such as $\leq 10\%$ or
 $\leq 5\%$ or $\leq 3\%$ with lower limits being $\leq 0.05\%$ or 0.1% (all in w/v-%). The
term "volatile" for solvents typically means boiling points of $\leq 200^\circ\text{C}$, such
10 as $\leq 150^\circ\text{C}$ or $\leq 100^\circ\text{C}$, at atmospheric pressure. Examples are inorganic
solvents and organic solvents with particular emphasis of dimethyl
sulfoxide and trifluoroethanol and mixtures thereof. The term solvent
includes mixtures of liquids which are miscible with each other. The
solutions may contain agents that enhance or diminish the solubility of the
15 PKI, e.g. acidic, alkaline, buffer components and/or other organic solvents.

Illustrative fluids which can be used as an antisolvent are

- a) gaseous at room temperature and atmospheric pressures, or
- b) liquid at room temperature and atmospheric pressure.

20

The antisolvent is typically selected for its ability to be readily dispersed
into small droplets and for its ability to act as an atomizing agent and
antisolvent against the PKI present in the solution.

25 Compounds/elements according to group (a) may be selected from carbon
dioxide ($P_c = 74\text{ bar}$ and $T_c = 31^\circ\text{C}$) (preferred), nitrous oxide ($P_c = 72$
bar and $T_c = 36^\circ\text{C}$), sulphur hexafluoride ($P_c = 37\text{ bar}$ and $T_c = 45^\circ\text{C}$),
ethane ($P_c = 48\text{ bar}$ and $T_c = 32^\circ\text{C}$), ethylene ($P_c = 51\text{ bar}$ and $T_c =$
 10°C), xenon ($P_c = 58\text{ bar}$ and $T_c = 16^\circ\text{C}$), trifluoromethane ($P_c = 47\text{ bar}$
30 and $T_c = 26^\circ\text{C}$), chlorotrifluoromethane ($P_c = 39\text{ bar}$ and $T_c = 29^\circ\text{C}$) and
nitrogen ($P_c = 34\text{ bar}$ and $T_c = -147^\circ\text{C}$) and mixtures containing these
compounds/elements. P_c stands for critical pressure and T_c for critical

temperature. Compounds according to group (b) are typically selected amongst conventional liquids of the same general types as discussed for solvents above but with the difference that the PKI present in the solution must be poorly soluble in the antisolvent. Particular liquids of group (b) 5 comprise methanol, ethanol, acetone water and mixtures containing one or more of these fluids.

The antisolvents of group (a) above are typically used at pressures and temperatures providing i) supercritical conditions (supercritical fluid) or ii) a 10 subcritical conditions (subcritical fluid) in the particle formation function and/or upstream of this function, such as in the mixing function and upstream of this latter function.

Variant (i) means pressures and temperatures which are typically above 15 the critical pressure P_c and critical temperature T_c of the antisolvent used. For the pressure this typically means pressures in the interval $(1.0-7.0) \times P_c$ or in the interval ≥ 10 bar, suitably ≥ 20 bar with preference for ≥ 30 bar, higher than P_c with illustrative upper limits being 100 bar, 200 bar and 300 bar higher than P_c . For the temperature this typically means temperatures 20 within $(1.0-4.0) \times T_c$ or in the interval of $\geq 5^\circ\text{C}$, suitably $\geq 10^\circ\text{C}$ with preference for $\geq 15^\circ\text{C}$ above T_c with illustrative upper limits being 10°C , 40°C and 50°C above T_c .

Variant (ii) means that at least one of temperature and pressure, with 25 preference for only the temperature, is/are below the critical value. (T_c and P_c , respectively). Thus the temperature may be in the interval of $(0.1-1) \times T_c$, such as $(0.5-1) \times T_c$, or lower. Further, the temperature may be low, such as -10°C or -30°C . These temperatures may be combined with pressures as defined in the preceding paragraph or with pressures lower 30 than the P_c of the used antisolvent. For carbon dioxide this means that the temperature in the particle formation function is $< +31^\circ\text{C}$, such as about $+25^\circ\text{C}$ or lower combined with a pressure above or below 74 bar.

The antisolvents of group (b) above are typically used in the subcritical state, i.e. as a subcritical fluid.

- In one aspect of the invention, there is provided a pharmaceutical composition comprising stable, amorphous hybrid nanoparticles of at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component; which composition optionally further comprises at least one pharmaceutically acceptable solubilizer.
- 10 In one embodiment of this aspect, there is provided a pharmaceutical composition comprising stable, amorphous hybrid nanoparticles of at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component; which composition further comprises at least one pharmaceutically acceptable solubilizer. Typically, said solubilizer is present separated from the hybrid nanoparticles in the composition. Or,
- 15 typically, said solubilizer is distributed to the surface of the hybrid nanoparticles. Said solubilizer may be selected from polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer, d- α -tocopherol acid polyethylene glycol 1000 succinate and a hydrogenated castor oil, such as PEG-40 hydrogenated castor oil or PEG-35 hydrogenated castor oil. Furthermore, said solubilizer may be a poloxamer.
- 20

The compositions comprising stable, amorphous hybrid nanoparticles comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component, display increased dissolution rate.

25

Consequently, in another embodiment of this aspect, there is provided a composition comprising stable, amorphous hybrid nanoparticles, comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component, wherein said hybrid nanoparticles display an increased dissolution rate of said protein kinase

30

inhibitor, compared to the dissolution rate of said protein kinase inhibitor in raw, crystalline form.

Typically, said dissolution rate is measured by a flow through cell system in
5 sink conditions, e.g., according to the US Pharmacopeia (USP4).

Dissolution measurement in sink conditions of hybrid nanoparticles may be measured in a method consisting of adding the wished amount of powder into a flow through cell system (SOTAX, Allschwill, Switzerland), mounting the cell onto its apparatus and then pumping the appropriate medium
10 (typically FaSSIF, FeSSIF, SGF) through the powder. The temperature of the apparatus is typically set to 37°C. The amount of powder added into the cell depends on drug load of the powder: The exact amount of powder can be calculated from results obtained from drug load analysis of the powders. The PKI may be added into the flow through cell and a flow rate
15 between 5 and 25 ml medium/min is pumped through the powder. One ml samples of the medium passing through the cell is collected at predetermined times and subsequently analyzed by HPLC (e.g. C18 column Eclipse, 4.6 mm x 15 cm, 1 ml/min, detection 254 to 400 nm). Samples are typically taken after 0, 0.5, 1, 1.5, 2, 3, 4, 5, 6, 7, 8, 9, 10, 15,
20 20, 25, 30, 35 and 40 min from the moment the medium comes out from the flow through cell. The accumulated % solubilized of the amount of active substance added into the flow through cell can be calculated and plotted against time (min). The initial slope ("initial dissolution rate", representing 0-10 minutes) of the graph may be estimated and taken as
25 the dissolution rate of the material in sink condition at 37°C in the given dissolution medium.

Preferably, the dissolution rate is measured within the initial 0 to 10
30 minutes of dissolution.

The increased dissolution rate is preferably measured in a solution as a dissolution rate ratio of said stable, amorphous hybrid nanoparticles and

said protein kinase inhibitor in raw, crystalline form. Preferably said ratio is from about 1.5:1 to about 500:1, such as from about 10:1 to about 30:1.

Preferably, the dissolution rate is measured in a solution with intestinal pH,
5 such as FaSSIF or FeSSIF or in a solution with gastric pH, such as SGF.

Typically, said dissolution rate is measured by a flow through cell system, for instance in sink conditions. Dissolution measurement in sink conditions of stable, amorphous hybrid nanoparticles may be measured in a method
10 consisting of adding the wished amount of powder into a flow through cell system (SOTAX, Allschwill, Switzerland), mounting the cell onto its apparatus and then pumping the appropriate medium (typically FaSSIF, FeSSIF, SGF) through the powder. The temperature of the apparatus is typically set to 37°C. The amount of powder added into the cell depends
15 on drug load of the powder: The exact amount of powder can be calculated from results obtained from drug load analysis of the powders. The PKI may be added into the flow through cell and a flow rate between 5 and 25 ml medium/min is pumped through the powder. One ml samples of the medium passing through the cell is collected at predetermined times and
20 subsequently analyzed by HPLC (e.g. C18 column Eclipse, 4.6 mm x 15 cm, 1 ml/min, detection 254 to 400 nm). Samples are typically taken after 0, 0.5, 1, 1.5, 2, 3, 4, 5, 6, 7, 8, 9, 10, 15, 20, 25, 30, 35 and 40 min from the moment the medium comes out from the flow through cell. The accumulated % solubilized of the amount of active substance added into
25 the flow through cell, can be calculated and plotted against time (min). The initial slope ("initial dissolution rate", representing 0-10 minutes) of the graph can be estimated and taken as the dissolution rate of the material in sink condition at 37°C in the given dissolution medium.

30 In another embodiment of this aspect, there is provided a composition comprising stable, amorphous hybrid nanoparticles, comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and

matrix-forming component, which provides a solubility increase of inhibitor in a solution, said increase measured as the area under the curve (AUC) during about from 40 minutes to about 90 minutes, in said solution as compared with the AUC of inhibitor in raw, crystalline form. Typically, said
5 increase is from about 2:1 to about 10 000:1, wherein 1 represents AUC of inhibitor in raw, crystalline form. The increase may be measured in a solution with intestinal pH, such as FaSSIF or FeSSIF, or in a solution with gastric pH, such as SGF.

10 The polymeric stabilizing and matrix-forming component of the present invention includes, but not limited to, methyl cellulose, hydroxyethyl cellulose, hydroxypropyl cellulose (e.g. HPC ef, HPC lf and HPC jf), hydroxypropyl methylcellulose (e.g. Methocel E3 and E15 and
Pharmacoat), hydroxypropyl methylcellulose acetate succinate (HPMC
15 AS), hydroxypropyl methylcellulose phthalate (e.g. HPMCP HP55), polyvinylpyrrolidone (e.g. PVP 30K and PVP 90K), polyvinyl acetate phthalate (PVAP), copolyvidone (e.g. Kollidon VA 64), crospovidon (e.g. Kollidon CL), methacrylic acid and ethylacrylate copolymer (e.g. Kollicoat
ME), methacrylate acid and methyl methacrylate copolymer (e.g. Eudragit
20 L100), polyethylene glycol (PEG), DL lactide/glycolide copolymer, poly DL-lactide, cellulose acetate phthalate (CAP), carbomer homopolymer Type A (Carbopol 971P), carbomer homopolymer Type B (Carbopol 974P), aminoalkyl methacrylate copolymers (e.g. Eudragit RL100, RL PO or RS
PO) and Poloxamers (e.g. Pluronic, Kolliphor).

25

Consequently, in another embodiment of this aspect, said polymeric stabilizing and matrix-forming component is selected from from methyl cellulose, hydroxyethyl cellulose, hydroxypropyl cellulose, hydroxypropyl methylcellulose, hydroxypropyl methylcellulose acetate succinate,
30 hydroxypropyl methylcellulose phthalate, polyvinylpyrrolidone, polyvinyl acetate phthalate, copolyvidone, crospovidon, methacrylic acid and ethylacrylate copolymer, methacrylate acid and methyl methacrylate

copolymer, polyethylene glycol, DL lactide/glycolide copolymer, poly DL-lactide, cellulose acetate phthalate, carbomer homopolymer Type A, carbomer homopolymer Type B, aminoalkyl methacrylate copolymers and polaxamers. Preferably, said polymeric stabilizing and matrix-forming
5 component is selected from hydroxypropyl methylcellulose phthalate, hydroxypropyl cellulose, copolyvidon, hydroxypropyl methylcellulose acetate succinate, polyvinyl acetate phthalate, cellulose acetate phthalate and polyvinylpyrrolidone.

10 In another embodiment of this aspect, there is provided a composition comprising stable, amorphous hybrid nanoparticles comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component, characterized by providing an amorphous powder X-ray diffraction pattern.

15

In another embodiment of this aspect, there is provided a composition comprising stable, amorphous hybrid nanoparticles comprising at least one protein kinase inhibitor and at least one polymeric stabilizing and matrix-forming component, wherein the dissolution rate of said stable, amorphous
20 hybrid nanoparticles remain stable to at least about 90%, after 6 months of storage or more, at room temperature.

In another embodiment of this aspect, said protein kinase inhibitor is a tyrosine kinase inhibitor selected from the group consisting of lapatinib,
25 pazopanib, nilotinib, erlotinib, dasatinib, gefitinib, sorafenib, crizotinib, vemurafenib and axitinib; or salts or hydrates or solvates thereof, or combinations thereof. In some embodiments it may be advantageous to use other PKIs. Examples of PKI include, but are not limited to afatinib, bosutinib, cediranib, fostamatinib, imatinib, lenvatinib, lestaurtinib,
30 motesanib, mubritinib, pegaptanib, ruxolitinib, semaxanib, sunitinib, tandunitib, tipifamib and vandetanib; or salts or hydrates or solvates thereof, or combinations thereof.

In another embodiment of this aspect, said stable, amorphous hybrid nanoparticles has an average particle diameter size of less than about 1000 nm, such as less than about 500 nm, preferably less than 250 nm.

- 5 In another embodiment of this aspect, said solvent is an organic solvent selected from DMSO and trifluoroethanol, or a mixture of these solvents, or mixture of these solvents with other organic solvent such as DMSO/acetone, DMSO/tetrahydrofurane or trifluoroethanol/ethyl acetate.
- 10 The compositions of the present invention may also dissolve and the protein kinase inhibitor may be systemically absorbed independently of the pH in the surrounding environment, and typically approximately in equal amounts, especially at both a gastric pH, such as from about pH 1.2 to about pH 2.1, preferably about 1.7 and at a intestinal pH such as from
15 about pH 4.5 to about pH 8, preferably at a pH of about 6. With systemically absorbed, is meant that the protein kinase inhibitor is released from the stable, amorphous hybrid nanoparticles and taken up by the systemic blood stream. Therefore, in another embodiment of this aspect, there is provided a composition, wherein said protein kinase inhibitor is
20 systemically absorbed independently of the pH. Typically, said protein kinase inhibitor is systemically absorbed with approximately equal amounts at both a gastric pH and at an intestinal pH. Preferably, said acid pH is about pH 1.4 and preferably said neutral pH is about pH 6.5.
- 25 With approximately equal amounts is meant that the concentration of protein kinase inhibitor in the blood stream, after exposure is approximately similar. This may be illustrated by a ratio, wherein the concentration of protein kinase inhibitor in the blood stream is measured after administration in gastric pH conditions (A) and compared with the
30 concentration of protein kinase inhibitor in the blood stream is measured after administration in intestinal pH conditions (N). Typically, the ratio A:N is from about 0.75:1 to about 1.5:1 and preferably from about 1:1 to about 1.25:1. The concentration measurement of protein kinase inhibitor in the

blood stream may be carried out as an area under the curve (AUC) during 0-24 hours, the maximum concentration (C_{max}) or as bioavailability.

Consequently, in another embodiment of this aspect, there is provided a
5 composition comprising stable, amorphous hybrid nanoparticles,
comprising at least one protein kinase inhibitor and at least one polymeric
stabilizing and matrix-forming component, wherein the concentration of
systemically absorbed protein kinase inhibitor in gastric pH conditions
compared with the concentration of systemically absorbed protein kinase
10 inhibitor in intestinal pH conditions is in a ratio of from about 0.75:1 to
about 1.5:1, preferably of from about 1:1 to about 1.25:1. Typically said
gastric pH condition represents a pH of about 1.4 and said intestinal pH
condition represents a pH of about 6. Typically, the concentration is
measured as area under the curve (AUC) during 0-24 hours of exposure of
15 the composition or as the maximum concentration (C_{max}).

The amounts of systemically absorbed protein kinase inhibitor may be
measured in various ways. There is provided, in Example 14 in the present
disclosure, a method for measurement of systemically absorbed protein
20 kinase inhibitors at various pHs, i.e. under both acid and neutral
conditions.

In another embodiment of this aspect, there is provided a composition
comprising stable, amorphous hybrid nanoparticles, comprising at least
25 one protein kinase inhibitor and at least one polymeric stabilizing and
matrix-forming component, which produces a solubility increase of inhibitor
in a solution up to supersaturation, said increase measured as the area
under the curve (AUC) during about 90 minutes, in said solution and
compared with the AUC of inhibitor in crystalline form. Said increase may
30 be from to about 2:1 to about 1000:1, wherein 1 represents AUC of
inhibitor in crystalline form.

For understanding how the hybrid nanoparticles in the compositions of the invention will dissolve *in vivo* in the different environments of the stomach, small intestine, large intestine and colon, it is important to choose an appropriate solution for *in vitro* dissolution testing. It is critical that the *in vitro* test conditions mimic the *in vivo* environment as closely as possible, for example pH and osmolarity. Typically, for intestinal uptake, the pH is between 6 and 7. Therefore, the solution may hold a pH from about pH 6 to about pH 7, such as about pH 6.5.

10 Therefore, in embodiments of the invention, the solution for testing has a pH from about pH 4.5 to about pH 8, such as about pH 6.5 or such as about pH 5. The solutions may represent Fasted Simulated State Intestinal Fluid (FaSSIF) or Fed Simulated State Intestinal Fluid (FeSSIF).

15 Typically, for gastric uptake, the pH is between 1 and 2. Therefore, the solution may hold a pH from about pH 1 to about pH 2, such as about pH 1.4. Therefore, in embodiments of the invention, the solution for testing may represent Simulated Gastric Fluid (SGF).

20 The choice of solution will be dependent on where in the intestinal tract and under what conditions (fasted or fed) the composition is desired to dissolve and be taken up. Recipes and preparation of these solutions are obtainable from the manufacturer (Biorelevant, Croydon, U.K.). Further details are also disclosed in Jantratid, E., and Dressman, J. (2009) *Dissolut. Technol.* 8, 21-25).

The amount of PKI in the hybrid nanoparticles in the compositions of the present invention may be less or more, such as wherein the amount of PKI in the hybrid nanoparticles is from about 0.01% by weight to about 99.9% by weight.

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In another embodiment of this aspect, there is provided compositions comprising stable, amorphous hybrid nanoparticles of the present invention, wherein the amount of PKI in the hybrid nanoparticles is from about 10% by weight to about 70% by weight.

5

In another embodiment of this aspect, there is provided provided compositions comprising stable, amorphous hybrid nanoparticles of the present invention, wherein the amount of PKI in the hybrid nanoparticles is from about 10% by weight to about 50% by weight.

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In some embodiments, it may be advantageous that the amount of PKI in the stable, amorphous hybrid nanoparticles is from 5% by weight to about 50% by weight, from 10% by weight to about 40% by weight, from about 10% by weight to about 30% by weight, or from about 10 % by weight to about 20% by weight.

15

Control of the characteristics of the particles may be convenient for specific applications. Particle size, particle agglomeration, particles porosity and the choice and ratio of the polymeric stabilizing and matrix-forming agent could be modified in order to increase or decrease the surface area to volume ratio of the particle or behaviour of the particles in a gastrointestinal fluids, leading to an increase or decrease of the dissolution rate. Dependent on the desired dissolution characteristics such particles characteristics may be adapted. Furthermore, particles with different characteristics may be present in the same pharmaceutical composition to provide an initial dose and a prolonged or delayed dose of active ingredient. Additionally, it may be advantageous to provide different PKIs and/or other active ingredient(s) in different primary particles with different characteristics adapted to provide desired dissolution rates for each active ingredient(s).

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Other embodiments of the invention provide pharmaceutical compositions comprising the stable, amorphous hybrid nanoparticles. Such compositions may further comprise at least one pharmaceutically acceptable solubilizer. Said solubilizer may be present separated from the stable, amorphous
5 hybrid nanoparticles (i.e. physically mixed with pre-prepared solid nanoparticles) in the composition or be randomly intermixed within the stable, amorphous hybrid nanoparticles in the pharmaceutical composition. The pharmaceutical composition may also be in a dosage form consisting of several layers, for example laminated or multilayered tablets, such that
10 the hybrid nanoparticles are separated from the solubilizer. The solubilizer may be selected from polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer, d- α -tocopherol acid polyethylene glycol 1000 succinate and a hydrogenated castor oil, such as PEG-40 hydrogenated castor oil or PEG-35 hydrogenated castor oil. Said solubilizer may also be a
15 poloxamer.

In another embodiment of this aspect, said inhibitor is a tyrosine kinase inhibitor selected from the group consisting of lapatinib, pazopanib, nilotinib, erlotinib, dasatinib, gefitinib, sorafenib axitinib, crizotinib and vemurafenib; or salts or hydrates or solvates thereof, or combinations
20 thereof.

In another embodiment of this aspect, said inhibitor is nilotinib; and said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate or polyvinyl acetate phthalate.
25

In another embodiment of this aspect, said inhibitor is nilotinib; said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate or polyvinyl acetate phthalate; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol
30 copolymer or or d- α -tocopherol acid polyethylene glycol 1000 succinate.

In another embodiment of this aspect, said inhibitor is erlotinib, and said polymeric stabilizing and matrix-forming component is hydroxypropyl methylcellulose acetate succinate.

- 5 In another embodiment of this aspect, said inhibitor is erlotinib; said polymeric stabilizing and matrix-forming component is hydroxypropyl methylcellulose acetate succinate; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer or d- α -tocopherol acid polyethylene glycol 1000 succinate.

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In another embodiment of this aspect, said inhibitor is pazopanib; and said polymeric stabilizing and matrix-forming component is polyvinylpyrrolidone.

- 15 In another embodiment of this aspect, said inhibitor is pazopanib; said polymeric stabilizing and matrix-forming component is polyvinylpyrrolidone; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer or d- α -tocopherol acid polyethylene glycol 1000 succinate.

- 20 In another embodiment of this aspect, said inhibitor is lapatinib; and said polymeric stabilizing and matrix-forming component is hydroxypropyl cellulose.

- 25 In another embodiment of this aspect, said inhibitor is lapatinib; said polymeric stabilizing and matrix-forming component is hydroxypropyl cellulose; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer or d- α -tocopherol acid polyethylene glycol 1000 succinate.

- 30 In another embodiment of this aspect, said inhibitor is gefitinib; and said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate or polyvinyl acetate phthalate or polyvinylpyrrolidone.

In another embodiment of this aspect, said inhibitor is gefitinib; said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate or polyvinyl acetate phthalate or polyvinylpyrrolidone; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer.

In another embodiment of this aspect, said inhibitor is dasatinib; and said polymeric stabilizing and matrix-forming component is copolyvidone.

10 In another embodiment of this aspect, said inhibitor is dasatinib; said polymeric stabilizing and matrix-forming component is copolyvidone; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer.

15 In another embodiment of this aspect, said inhibitor is sorafenib; and said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate.

In another embodiment of this aspect, said inhibitor is sorafenib; said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer.

25 In another embodiment of this aspect, said inhibitor is nilotinib base; and said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate or polyvinyl acetate phthalate.

In another embodiment of this aspect, said inhibitor is nilotinib base; said polymeric stabilizing and matrix-forming component is hydroxy propyl methyl cellulose phthalate or polyvinyl acetate phthalate; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer.

In another embodiment of this aspect, said inhibitor is axitinib; and said polymeric stabilizing and matrix-forming component is copolyvidone or hydroxypropyl methylcellulose acetate succinate.

- 5 In another embodiment of this aspect, said inhibitor is axitinib; said polymeric stabilizing and matrix-forming component is copolyvidone or hydroxypropyl methylcellulose acetate succinate; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer.
- 10 In another embodiment of this aspect, said inhibitor is crizotinib; and said polymeric stabilizing and matrix-forming component is copolyvidone or polyvinylpyrrolidone.

- In another embodiment of this aspect, said inhibitor is crizotinib; said
15 polymeric stabilizing and matrix-forming component is copolyvidone or polyvinylpyrrolidone; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer or PEG-40 hydrogenated castor oil.

- In another embodiment of this aspect, said inhibitor is vemurafenib; and
20 said polymeric stabilizing and matrix-forming component is copolyvidone or cellulose acetate phthalate.

- In another embodiment of this aspect, said inhibitor is vemurafenib; said
polymeric stabilizing and matrix-forming component is copolyvidone or
25 cellulose acetate phthalate; and said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol.

- In another embodiment of this aspect, said protein kinase inhibitor is
partially released from the composition, at a pH of from about 1 to about 2,
30 preferably at about pH 1.4.

- In another aspect of the invention, there is provided stable, amorphous
hybrid nanoparticles, comprising at least one protein kinase inhibitor and at
least one polymeric stabilizing and matrix-forming component, as defined
35 in the present disclosure.

In another embodiment of this aspect, there is provided a composition of the invention, for use in therapy.

- 5 In another embodiment of this aspect, there is provided a composition of the invention, for use in the treatment of proliferative disorders. Typically, said proliferative disorder is selected from tumours and cancers, including, but not limited to, neurofibromatosis, tuberous sclerosis, hemangiomas and lymphangiogenesis, cervical, anal and oral cancers, eye or ocular
- 10 cancer, stomach cancer, colon cancer, bladder cancer, rectal cancer, liver cancer, pancreas cancer, lung cancer, breast cancer, cervix uteri cancer, corpus uteri cancer, ovary cancer, prostate cancer, testis cancer, renal cancer, brain cancer, cancer of the central nervous system, head and neck cancer, throat cancer, skin melanoma, acute lymphocytic leukemia, acute
- 15 myelogenous leukemia, Ewing's Sarcoma, Kaposi's Sarcoma, basal cell carcinoma and squamous cell carcinoma, small cell lung cancer, choriocarcinoma, rhabdomyosarcoma, angiosarcoma, hemangioendothelioma, Wilms Tumor, neuroblastoma, mouth/pharynx cancer, esophageal cancer, larynx cancer, lymphoma, multiple myeloma;
- 20 cardiac hypertrophy, age-related macular degeneration and diabetic retinopathy.

In another embodiment of this aspect, there is provided a composition of the invention, said composition is provided during food intake.

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- In another aspect of the invention, there is provided a method of treating proliferative disorder in a patient in need thereof, comprising administering a therapeutically effective amount of a composition according to the present invention. Said proliferative disorder is typically selected from
- 30 tumours and cancers including, but not limited to, neurofibromatosis, tuberous sclerosis, hemangiomas and lymphangiogenesis, cervical, anal and oral cancers, eye or ocular cancer, stomach cancer, colon cancer, bladder cancer, rectal cancer, liver cancer, pancreas cancer, lung cancer, breast cancer, cervix uteri cancer, corpus uteri cancer, ovary cancer,

- prostate cancer, testis cancer, renal cancer, brain cancer, cancer of the central nervous system, head and neck cancer, throat cancer, skin melanoma, acute lymphocytic leukemia, acute myelogenous leukemia, Ewing's Sarcoma, Kaposi's Sarcoma, basal cell carcinoma and squamous
- 5 cell carcinoma, small cell lung cancer, choriocarcinoma, rhabdomyosarcoma, angiosarcoma, hemangioendothelioma, Wilms Tumor, neuroblastoma, mouth/pharynx cancer, esophageal cancer, larynx cancer, lymphoma, multiple myeloma; cardiac hypertrophy, age-related macular degeneration and diabetic retinopathy.
- 10 It will be appreciated that the amount of a protein kinase inhibitor in the stable, amorphous hybrid nanoparticles of the present invention required for use in treatment will vary not only with the particular inhibitor selected but also with the route of administration, the nature of the condition for which treatment is required and the age, weight and condition of the
- 15 patient and will be ultimately at the discretion of the attendant physician. In general however a suitable dose may be in the range of from about 0.005 to about 30 mg/kg of body weight per day, preferably in the range of 0.05 to 10 mg/kg/day.

The desired dose is conveniently presented in a single dose or as a

20 divided dose administered at appropriate intervals, for example as two, three, four or more doses per day. Dependent on the need of the treatment and/or prevention, the desired dose may also be, for example, once every two days, once every three days, or even once a week.

The composition is conveniently administered in unit dosage form; for

25 example containing 0.5 to 1500 mg, conveniently 1 to 1000 mg, most conveniently 5 to 700 mg of active ingredient per unit dosage form. The compositions of the invention will normally be administered via the oral, parenteral, intravenous, intramuscular, subcutaneous or other injectable ways, buccal, rectal, vaginal, transdermal and/or nasal route and/or via

30 inhalation, in a pharmaceutically acceptable dosage form. Depending upon

the disorder and patient to be treated and the route of administration, the compositions may be administered at varying doses.

Pharmaceutical compositions include but are not limited to those suitable for oral, rectal, nasal, topical (including buccal and sub-lingual),
5 transdermal, vaginal or parenteral (including intramuscular, subcutaneous and intravenous) administration or in a form suitable for administration by inhalation or insufflation. The compositions may, where appropriate, be conveniently presented in discrete dosage units and may be prepared by any of the methods well known in the art of pharmacy. Pharmaceutical
10 compositions suitable for oral administration are conveniently presented as discrete units such as capsules, cachets or tablets, each containing a predetermined amount of the active substance.

Tablets and capsules for oral administration may contain conventional excipients such as binding agents, fillers, lubricants, disintegrants, or
15 wetting agents. The tablets may be coated according to methods well known in the art.

The compositions may be formulated for parenteral administration (e.g. by injection, for example bolus injection or continuous infusion) and may be presented in unit dose form in ampoules, pre-filled syringes, small volume
20 infusion or in multi-dose containers with an added preservative. The compositions may take such forms as suspensions, solutions, or emulsions in oily or aqueous vehicles, and may contain formulation agents such as suspending, stabilizing and/or dispersing agents.

The above described compositions may be adapted to give sustained
25 release of the active inhibitor.

The following examples are provided to illustrate various embodiments of the present invention and shall not be considered as limiting in scope.

Examples

Below follows a number of non-limiting examples of compositions comprising stable, amorphous hybrid nanoparticles. In the tables, the following abbreviations to “compositions” apply:

- 5 “I” represents the protein kinase inhibitor (PKI);
“P” represents the polymeric stabilizing and matrix-forming component;
“S” represents the solubilizer;
“I+P” represents a physical mix of the inhibitor with the polymeric stabilizing and matrix-forming component, i.e. without further processing;
10 “I+S” represents a physical mix of the inhibitor with the solubilizer;
“I+P+S” represents a physical mix of the inhibitor, the polymeric stabilizing and matrix-forming component and the solubilizer;
“I/P” represents stable, amorphous hybrid nanoparticles with the inhibitor and the polymeric stabilizing and matrix-forming component;
15 “I/P+S” represents stable, amorphous hybrid nanoparticles with the inhibitor and the polymeric stabilizing and matrix-forming component and a separate solubilizer added;
“I/P/S” represents stable, amorphous hybrid nanoparticles with the inhibitor, the polymeric stabilizing and matrix-forming component and the
20 solubilizer.
“Exp” represents the experiment number.

The stable, amorphous hybrid nanoparticles were produced with exemplary PKIs, polymeric stabilizing and matrix-forming components
25 (“Polymers”), solubilizers, solution concentrations, ratios, solvents, antisolvents, temperatures and pressures as set out below and in Table A.

A 3-6 % w/v PKI / polymer solution in solvent, with a ratio PKI/polymer of about 20-70% w/w, was pumped through XSpray’s RightSize nozzle at the
30 flow rate of 1 ml/min using a high-performance liquid chromatography pump, together with a 100 g/min CO₂ (super- or subcritical) stream. The pressure in the precipitation chamber was set to about 100 – 175 bar and

the temperature was set to about 10 to 50°C. Both streams contact within the nozzle and the hybrid nanoparticles were formed and subsequently collected in the particle in the collecting chamber. The CO₂ and solvent passed through the filtering system of the collecting chamber and were drained via the back pressure regulator outlet which maintains the pressure within the precipitation and collecting chambers. After pumping of the PKI/polymer solution and cleaning of the tubing with the same solvent used to prepare the PKI/polymer solution, residual solvents left within both the precipitation and collecting chambers were removed by flushing these chambers with pure scCO₂. After the flushing process, the CO₂ was slowly drained off from the collecting chamber. Once the CO₂ had been completely removed, the particles on the filtering system were collected for analysis.

For I/P/S type particles, a defined amount of solubilizer is added and dissolved into the PKI/polymer solution before pumping the solution through the nozzle for precipitation according to the methods described above.

For I/P+S type particles, a defined amount of solubilizer is added to the stable, amorphous hybrid nanoparticles in a glass vial. The glass vial is slowly rotated for mixing of the solubilizer with the hybrid nanoparticles.

Table A Stable, amorphous hybrid nanoparticles with exemplary PKIs, polymeric stabilizing and matrix-forming components, solvents, antisolvents and conditions.

PKI/Polymer	Exp. #	Solution conc. % (w/v)	Ratio PKI/Polymer % (w/w)	Solvent & Antisolvent	Temperature & Pressure
Axitinib /Kollidon VA64	160, 162 & 581	5%	25%	DMSO & CO ₂	25°C & 125 Bars
Crizotinib /PVP 30K	153, 155, 156 & 571	5%	25%	DMSO & CO ₂	25°C & 125 Bars
Dasatinib /Kollidon VA64	140, 141 & 551	4%	35%	DMSO/Acetone (1:2) & CO ₂	15°C & 125 Bars

Erlotinib HCl /HPMC AS	511	3.6%	35%	TFE & CO ₂	25°C & 150 Bars
Gefitinib /HPMCP HP55	135, 137 & 541	4%	35%	DMSO/Acetone (1:2) & CO ₂	40°C & 150 Bars
Lapatinib base /HPC If	531	5%	66%	DMSO/Acetone (1:2) & CO ₂	40°C & 150 Bars
Nilotinib base /HPMCP HP55	501	5%	40%	TFE & CO ₂	15°C & 125 Bars
Pazopanib HCl /PVP 90K	521	3.6%	35%	TFE & CO ₂	25°C & 150 Bars
Sorafenib tosylate /HPMCP HP55	561	4%	35%	DMSO/Acetone (1:2) & CO ₂	40°C & 150 Bars
Vemurafenib /CAP	168, 170 & 592	5%	25%	DMSO & CO ₂	25°C & 125 Bars

General description of dissolution measurement assay

- The method consists of adding the wished amount of powder of stable, amorphous hybrid nanoparticles into a glass vial and then pouring in it the appropriate medium (typically FaSSIF, FeSSIF or SGF). The medium was prepared in accordance with the manufacturer's instructions. The amount of powder added depends on the wished "total PKI concentration". For some experiments where powders with high drug loads were tested and compared, the real amount of PKI in the stable, amorphous hybrid nanoparticles was not taken in account. For other experiments, the drug load was first estimated by HPLC and the amount of powder to obtain the drug concentration was calculated.
- Typically, the powder was added in a 8 mL glass bottle and 7 mL of solution was added (typically FaSSIF, FeSSIF or SGF). The glass bottle was put on a shaker (approximately 1 rotation per minute) for dissolution. Samples of 500 µl where taken after different times, and subsequently centrifuged at approximately 15000 g for 3 minutes. The resulting supernatant was then analyzed by HPLC (C₁₈ column Eclipse, 4.6 mm x 15 cm, 1mL/min, detection at 254-400 nM. Generally samples were taken after 5, 30 and 90 min and eventually 150 min.

Example 1. Compositions with stable, amorphous hybrid nanoparticles with nilotinib – solubility at pH 6.5 and pH 5.

A number of experiments were carried out, wherein nilotinib base or nilotinib HCl represented the protein kinase inhibitor. The experiments were carried out by measuring concentration of solubilized PKI (mg/L) after 5, 30 and 90 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Further, experiments were carried out in an alternative solution at about pH 5, namely FeSSIF (Fed State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of protein kinase inhibitor was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 1 and 2, where Table 1 provides data of concentration of nilotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution, whereas Table 2 provides data of % solubilized nilotinib HCl after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase of stable, amorphous hybrid nanoparticles, compared to nilotinib HCl in raw, crystalline form added to the solution (experiments 1-40). In Tables 3 and 4, there is provided dissolution data in FeSSIF solution, presented similarly as Table 1 and 2 (experiments 41-55). Table 5 provides data from a comparative experiment with similar stable, amorphous hybrid nanoparticles, carried out in FaSSIF and FeSSIF, respectively (experiments 56-57). Table 6 presents further comparative data for experiments carried out in FaSSIF and FeSSIF, respectively.

Table 1. Nilotinib - concentration of nilotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
1	I	Nilotinib HCl (raw) 100 mg	100	-	-	0.1	0.2	0.1
2	I	Nilotinib HCl (raw) 500 mg	100	-	-	0.2	0.2	0.2

3	I	Nilotinib HCl (raw) 1000 mg	100	-	-	0.2	0.3	0.2
4	I	Nilotinib Base (raw) 500 mg	100	-	-	0.6	0.5	0.2
5	I+P	Nilotinib HCl (raw) 1000 mg	100	HPMCP HP55 2000 mg	-	0.2	0.5	0.5
6	I+P	Nilotinib HCl (raw) 1000 mg	100	PVAP 2000 mg	-	1.3	0.2	0.4
7	I+P	Nilotinib HCl (raw) 1000 mg	100	Eudragit L100 2000 mg	-	0.2	0.4	0.2
8	I+P	Nilotinib HCl (raw) 1000 mg	100	Methocel E15 2000 mg	-	0.1	0.1	0.1
9	I+S	Nilotinib HCl (raw) 1000 mg	100	-	Soluplus 357.5 mg	0.4	0.3	0.4
10	I+S	Nilotinib HCl (raw) 1000 mg	100	-	Soluplus 715 mg	0.4	0.5	0.5
11	I+S	Nilotinib HCl (raw) 1000 mg	100	-	Soluplus 1072 mg	0.4	0.5	0.6
12	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	0.4	0.6	1.0
13	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	Soluplus 715 mg	0.2	0.2	0.3
14	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	TPGS 1000 mg	0.5	0.9	1.1
15	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	TPGS 1000 mg	0.2	0.4	0.5
16	I+P+S	Nilotinib Base (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	0.2	0.5	0.4
17	I/P	Nilotinib HCl 100 mg	50	HPMCP HP55 100 mg	-	9.5	5.6	4.5
18	I/P	Nilotinib HCl 100 mg	40	HPMCP HP55 150 mg	-	10.4	5.0	3.7
19	I/P	Nilotinib HCl 100 mg	50	PVAP 100 mg	-	7.3	5.0	4.1
20	I/P	Nilotinib HCl 100 mg	40	PVAP 150 mg	-	8.7	5.0	3.4
21	I/P	Nilotinib HCl 100 mg	50	Methocel E15 100 mg	-	1.4	1.5	1.8
22	I/P	Nilotinib HCl 100 mg	50	Eudragit L100 100 mg	-	5.1	5.9	4.9
23	I/P	Nilotinib Base 100 mg	40	HPMCP HP55 150 mg	-	9.7	4.7	3.8
24	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	Soluplus 715 mg	53.4	46.1	35.6
25	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	Soluplus 1430 mg	85.9	87.9	80.8
26	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	Soluplus 2145 mg	117.0	127.1	116.9
27	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	TPGS 1000 mg	49.6	30.1	22.3
28	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	TPGS 2000 mg	98.4	57.4	42.6
29	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 357.5 mg	93.5	45.2	14.1
30	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	145.0	134.3	36.8
31	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	TPGS 1000 mg	93.8	31.0	22.4
32	I/P+S	Nilotinib HCl	40	PVAP	Soluplus	82.9	137.9	42.9

		500 mg		750 mg	715 mg			
33	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	TPGS 1000 mg	77.8	32.3	22.8
34	I/P+S	Nilotinib HCl 500 mg	50	Methocel E15 500 mg	Soluplus 715 mg	3.3	4.0	5.8
35	I/P+S	Nilotinib HCl 500 mg	50	Methocel E15 500 mg	TPGS 1000 mg	4.8	5.4	6.7
36	I/P+S	Nilotinib Base 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	178.1	120.4	33.7
37	I/P/S	Nilotinib HCl 500 mg	25.4	HPMCP HP55 750 mg	Soluplus 715 mg	25.9	15.8	16.3
38	I/P/S	Nilotinib HCl 500 mg	25.4	PVAP 750 mg	Soluplus 715 mg	9.5	13.2	10.1
39	I/P/S	Nilotinib HCl 500 mg	22.2	HPMCP HP55 750 mg	TPGS 1000 mg	16.2	13.7	3.9
40	I/P/S	Nilotinib HCl 500 mg	22.2	PVAP 750 mg	TPGS 1000 mg	13.3	12.1	9.7

Table 2. Percentage solubilized nilotinib HCl after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase of compositions comprising stable, amorphous

5 hybrid nanoparticles with nilotinib, compared to nilotinib HCl in raw, crystalline form added to the FaSSiF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solub- ilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
1	I	Nilotinib HCl (raw) 100 mg	100	-	-	0.20	13.0	-
2	I	Nilotinib HCl (raw) 500 mg	100	-	-	0.04	23.5	-
3	I	Nilotinib HCl (raw) 1000 mg	100	-	-	0.03	21.8	-
4	I	Nilotinib Base (raw) 500 mg	100	-	-	0.50	36.5	-
5	I+P	Nilotinib HCl (raw) 1000 mg	100	HPMCP HP55 2000 mg	-	0.05	39.3	2.0
6	I+P	Nilotinib HCl (raw) 1000 mg	100	PVAP 2000 mg	-	0.02	40.0	2.1
7	I+P	Nilotinib HCl (raw) 1000 mg	100	Eudragit L100 2000 mg	-	0.04	26.0	1.3
8	I+P	Nilotinib HCl (raw) 1000 mg	100	Methocel E15 2000 mg	-	0.01	8.8	0.5
9	I+S	Nilotinib HCl (raw) 1000 mg	100	-	Soluplus 357.5 mg	0.03	30.8	1.6
10	I+S	Nilotinib HCl (raw) 1000 mg	100	-	Soluplus 715 mg	0.05	42.3	2.2
11	I+S	Nilotinib HCl (raw) 1000 mg	100	-	Soluplus 1072 mg	0.05	45.3	2.3
12	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	0.12	61.5	3.2
13	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	Soluplus 715 mg	0.04	20.5	1.1
14	I+P+S	Nilotinib HCl	100	HPMCP HP55	TPGS	0.18	78.8	4.1

		(raw) 500 mg		750 mg	1000 mg			
15	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	TPGS 1000 mg	0.08	35.0	1.8
16	I+P+S	Nilotinib Base (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	0.10	36.3	1.9
17	I/P	Nilotinib HCl 100 mg	50	HPMCP HP55 100 mg	-	5.6	515.5	26.6
18	I/P	Nilotinib HCl 100 mg	40	HPMCP HP55 150 mg	-	5.0	479.5	24.7
19	I/P	Nilotinib HCl 100 mg	50	PVAP 100 mg	-	5.0	445.0	22.9
20	I/P	Nilotinib HCl 100 mg	40	PVAP 150 mg	-	5.0	445.0	22.9
21	I/P	Nilotinib HCl 100 mg	50	Methocel E15 100 mg	-	1.5	138.8	7.2
22	I/P	Nilotinib HCl 100 mg	50	Eudragit L100 100 mg	-	5.9	474.3	24.2
23	I/P	Nilotinib Base 100 mg	40	HPMCP HP55 150 mg	-	4.7	459.3	23.7
24	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	Soluplus 715 mg	9.2	3828.3	197.3
25	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	Soluplus 1430 mg	17.6	7448.3	383.9
26	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	Soluplus 2145 mg	25.4	10663.8	549.7
27	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	TPGS 1000 mg	6.0	2692.3	138.8
28	I/P+S	Nilotinib HCl 500 mg	50	HPMCP HP55 500 mg	TPGS 2000 mg	11.5	5193.5	267.7
29	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 357.5 mg	9.0	3746.5	193.1
30	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	26.9	8974.8	462.6
31	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	TPGS 1000 mg	6.2	3396.5	175.1
32	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	Soluplus 715 mg	27.6	8391.3	432.5
33	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	TPGS 1000 mg	6.5	3223.8	166.2
34	I/P+S	Nilotinib HCl 500 mg	50	Methocel E15 500 mg	Soluplus 715 mg	0.8	393.5	20.3
35	I/P+S	Nilotinib HCl 500 mg	50	Methocel E15 500 mg	TPGS 1000 mg	1.1	505.5	25.9
36	I/P+S	Nilotinib Base 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	24.1	8799.5	453.6
37	I/P/S	Nilotinib HCl 500 mg	25.4	HPMCP HP55 750 mg	Soluplus 715 mg	3.2	1549.0	79.8
38	I/P/S	Nilotinib HCl 500 mg	25.4	PVAP 750 mg	Soluplus 715 mg	2.6	1006.5	51.9
39	I/P/S	Nilotinib HCl 500 mg	22.2	HPMCP HP55 750 mg	TPGS 1000 mg	2.7	942.3	48.6
40	I/P/S	Nilotinib HCl 500 mg	22.2	PVAP 750 mg	TPGS 1000 mg	2.4	1004.8	51.8

Table 3. Nilotinib - concentration of nilotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution in FeSSIF solution (pH 5).

Exp	Comp.	Inhibitor (I)	Drug	Polymeric	Solubilizer	Conc	Conc	Conc
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			load ratio (%)	stab. matrix. Component (P)	(S)	(mg/L) 5 min	(mg/L) 30 min	(mg/L) 90 min
41	I	Nilotinib HCl (raw) 500 mg	100	-	-	0.6	0.9	0.9
42	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	0.4	0.6	1.0
43	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 1000 mg	0.2	0.2	0.3
44	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	Soluplus 715 mg	0.5	0.9	1.1
45	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	TPGS 1000 mg	0.2	0.4	0.5
46	I/P	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	-	16.2	45.6	63.3
47	I/P	Nilotinib HCl 500 mg	40	PVAP 150 mg	-	3	7.7	11.2
48	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	47.7	85.5	109.4
49	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	TPGS 1000 mg	74.8	112.4	125.5
50	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	Soluplus 715 mg	12.9	21.3	27.3
51	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	TPGS 1000 mg	20.5	29.8	31.8
52	I/P/S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	42.3	81.5	108.1
53	I/P/S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	TPGS 1000 mg	86.3	116.3	128.8
54	I/P/S	Nilotinib HCl 500 mg	40	PVAP 750 mg	Soluplus 715 mg	6.3	18.8	28.2
55	I/P/S	Nilotinib HCl 500 mg	40	PVAP 750 mg	TPGS 1000 mg	20.5	29.8	31.8

Table 4. Percentage solubilized nilotinib HCl after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase of compositions comprising stable, amorphous

5 hybrid nanoparticles with nilotinib, compared to nilotinib HCl in raw, crystalline form added to the FeSSIF solution (pH 5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solub- ilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
41	I	Nilotinib HCl (raw) 500 mg	100	-	-	0.18	74.3	-
42	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	0.12	61.5	0.8
43	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 1000 mg	0.04	20.5	0.3
44	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	Soluplus 715 mg	0.18	78.8	1.1
45	I+P+S	Nilotinib HCl (raw) 500 mg	100	PVAP 750 mg	TPGS 1000 mg	0.08	35.0	0.5
46	I/P	Nilotinib HCl	40	HPMCP HP55	-	9.1	4080.0	54.9

		500 mg		750 mg				
47	I/P	Nilotinib HCl 500 mg	40	PVAP 150 mg	-	7.7	708.3	9.5
48	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	17.1	7631.3	102.8
49	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	TPGS 1000 mg	22.5	9664.0	130.2
50	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	Soluplus 715 mg	4.3	1917.8	25.8
51	I/P+S	Nilotinib HCl 500 mg	40	PVAP 750 mg	TPGS 1000 mg	6.0	2528.0	34.0
52	I/P/S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	16.3	7341.3	98.9
53	I/P/S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	TPGS 1000 mg	23.3	10101.3	136.0
54	I/P/S	Nilotinib HCl 500 mg	40	PVAP 750 mg	Soluplus 715 mg	3.8	1739.5	23.4
55	I/P/S	Nilotinib HCl 500 mg	40	PVAP 750 mg	TPGS 1000 mg	6.0	2528.0	34.0

Table 5. Nilotinib - concentration of nilotinib HCl (mg/L) after 5, 30, 90 and 150 minutes dissolution in FaSSIF and FeSSIF solution, respectively.

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilize r (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min	Conc (mg/L) 150 min
56 FaSSIF	I/P+S	Nilotinib HCl 75 mg	40	HPMCP HP55 112.5 mg	Soluplus 715 mg	51.2	66	62.3	53.2
57 FeSSIF	I/P+S	Nilotinib HCl 75 mg	40	HPMCP HP55 112.5 mg	Soluplus 715 mg	24.8	43.1	50.7	53

- 5 **Table 6.** Nilotinib - concentration of nilotinib HCl (mg/L) after 5, 30, 90 and 150 minutes dissolution in FaSSIF and FeSSIF solution, respectively presented as comparative data.

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilize r (S)	Compar e (%) 5 min	Compar e (%) 30 min	Compar e (%) 90 min	Comp are (%) 150 min
2 & 41	I	Nilotinib HCl (raw) 1000 mg	100	-	-	300	450	225	-
12 & 42	I+P+S	Nilotinib HCl (raw) 500 mg	100	HPMCP HP55 750 mg	Soluplus 715 mg	100	200	250	-
18 & 46	I/P	Nilotinib HCl 100/500 mg	40	HPMCP HP55 150/750 mg	-	156	912	1711	-
30 & 48	I/P+S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	33	64	301	-
56 & 57	I/P+S	Nilotinib HCl (raw) 75 mg	40	HPMCP HP55 112.5 mg	Soluplus 715 mg	48	65	81	100

37 & 52	I/P/S	Nilotinib HCl 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	163	516	663	-
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Conclusions Example 1

Experiments 17-23 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles with nilotinib HCl and a polymeric stabilizing and matrix-forming component. Particular improvements are achieved with the polymeric stabilizing and matrix-forming components hydroxypropyl methylcellulose phthalate (HPMCP HP55) and polyvinyl acetate phthalate (PVAP). These improvements are not obtained when physically mixing nilotinib HCl with a polymeric stabilizing and matrix-forming component. Experiments 24-36 clearly shows that a further solubility increase is obtained with stable, amorphous hybrid nanoparticles with nilotinib HCl and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added. Particular improvements are achieved by the addition of a separate solubilizer such as polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus) or d- α -tocopherol acid polyethylene glycol 1000 succinate (TPGS). These improvements were not obtained when physically mixing nilotinib HCl, solubilizer and/or polymeric stabilizing and matrix-forming component (I+S or I+P+S). No particular improvements were obtained with stable, amorphous hybrid nanoparticles with nilotinib HCl, a polymeric stabilizing and matrix-forming and a solubilizer (I/P/S).

The results carried out in FaSSIF and FeSSIF, respectively, indicate that the stable, amorphous hybrid nanoparticles of the invention provide a similar increase in solubility. One issue with PKI formulation is the food effect. Several of the PKIs are labeled for administration in fasted state despite the fact that food in most cases increases their bioavailability. Low bioavailability might partly explain the digestive problems that are associated with the PKIs. The similar dissolution rate in FaSSIF and FeSSIF indicates that the stable, amorphous hybrid nanoparticles of the invention (e.g. experiments 56/57) may reduce food effect and patient digestive problems by its solubility improvement that allows reducing

dosage. Thus stable, amorphous hybrid nanoparticles of the invention may be given in conjunction with food intake.

Example 2. Compositions with stable, amorphous hybrid

5 nanoparticles with erlotinib HCl – solubility at pH 6.5 and pH 5.

A number of experiments were carried out, wherein erlotinib HCl represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 5, 30 and 90 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated

10 Intestinal Fluid). Further, experiments were carried out in an alternative solution at about pH 5, namely FeSSIF (Fed State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

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Representative results in FaSSIF solution are provided below in Table 7 and 8, where Table 7 provides data of concentration of erlotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution, whereas Table 8 provides data of % solubilized erlotinib HCl after 30 minutes dissolution, the Area Under the

20 Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase of stable, amorphous hybrid nanoparticles, compared to erlotinib HCl in raw, crystalline form added to the solution (experiments 58-68). In Tables 9 and 10, there is provided dissolution data in FeSSIF solution, presented similarly as Table 7 and 8 (experiments 69-73). In Table 11,

25 data from a comparative experiment with similar stable, amorphous hybrid nanoparticles, carried out in FaSSIF and FeSSIF, respectively (experiments 74-83). Table 12 presents further comparative data for experiments carried out in FaSSIF and FeSSIF, respectively.

30 Table 7. Erlotinib - concentration of erlotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load	Polymeric stab. matrix.	Solubilizer (S)	Conc (mg/L)	Conc (mg/L)	Conc (mg/L)
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			ratio (%)	Component (P)		5 min	30 min	90 min
58	I	Erlotinib HCl (raw) 1000 mg	100	-	-	28.9	6.25	4.6
59	I+P	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 2000 mg	-	23	53.2	84
60	I+S	Erlotinib HCl (raw) 1000 mg	100	-	Soluplus 715 mg	92.8	156.6	176
61	I+S	Erlotinib HCl (raw) 1000 mg	100	-	TPGS 1000 mg	51.4	14.7	11.6
62	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	Soluplus 715 mg	96.7	256.6	361.8
63	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	TPGS 1000 mg	81.3	188.1	256.6
64	I/P	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	-	83.4	79.6	44.8
65	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 715 mg	187.3	269.7	284
66	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	TPGS 1000 mg	155.2	210.6	225.3
67	I/P/S	Erlotinib HCl 1000 mg	28	HPMC-AS 1850 mg	Soluplus 715 mg	90.1	95	96.4
68	I/P/S	Erlotinib HCl 1000 mg	26	HPMC-AS 1850 mg	TPGS 1000 mg	93.7	85.4	52.8

Table 8. Percentage solubilized erlotinib HCl after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase of stable, amorphous hybrid nanoparticles,

5 compared to erlotinib in raw, crystalline form added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
58	I	Erlotinib HCl (raw) 1000 mg	100	-	-	0.6	837	-
59	I+P	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 2000 mg	-	5.3	5126	6.1
60	I+S	Erlotinib HCl (raw) 1000 mg	100	-	Soluplus 715 mg	15.7	13328	15.9
61	I+S	Erlotinib HCl (raw) 1000 mg	100	-	TPGS 1000 mg	1.5	1744	2.1
62	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	Soluplus 715 mg	25.7	23210	27.7
63	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	TPGS 1000 mg	18.8	16912	20.2
64	I/P	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	-	8.0	5978	7.1
65	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 715 mg	27.0	22792	27.2
66	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	TPGS 1000 mg	21.1	18038	21.5
67	I/P/S	Erlotinib HCl 1000 mg	28	HPMC-AS 1850 mg	Soluplus 715 mg	9.5	8281	9.9

68	I/P/S	Erlotinib HCl 1000 mg	26	HPMC-AS 1850 mg	TPGS 1000 mg	8.5	6619	7.9
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Table 9. Erlotinib - concentration of erlotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution in FeSSIF solution (pH 5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
69	I	Erlotinib HCl (raw) 1000 mg	100	-	-	156.8	189.9	196
70	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	Soluplus 715 mg	25.5	75.1	126.2
71	I/P	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	-	258.2	402.1	464.5
72	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 715 mg	260.1	422.8	498.8
73	I/P/S	Erlotinib HCl 1000 mg	28	HPMC-AS 1850 mg	Soluplus 715 mg	293.6	395.2	434.9

- 5 **Table 10.** Percentage solubilized erlotinib HCl after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase of stable, amorphous hybrid nanoparticles, compared to erlotinib in raw, crystalline form added to the FeSSIF solution (pH 5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solub- ilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
69	I	Erlotinib HCl (raw) 1000 mg	100	-	-	19.0	16303	-
70	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	Soluplus 715 mg	7.5	7360	0.5
71	I/P	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	-	40.2	34897	2.1
72	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 715 mg	42.3	36835	2.3
73	I/P/S	Erlotinib HCl 1000 mg	28	HPMC-AS 1850 mg	Soluplus 715 mg	35.5	34244	2.1

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Table 11. Erlotinib - concentration of erlotinib HCl after 5, 30 and 90 minutes dissolution in FaSSIF and FeSSIF solution, respectively.

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
74 FaS SIF	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	Soluplus 1430 mg	134.1	369.8	533.4
75	I+P+S	Erlotinib HCl	100	HPMC-AS	Soluplus	24.4	88.8	154.4

FeS SIF		(raw) 1000 mg		1850 mg	1430 mg			
76 FaS SIF	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 1430 mg	275.4	441.4	508
77 FeS SIF	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 1430 mg	292.2	476.2	546.5
78 FaS SIF	I/P/S	Erlotinib HCl 1000 mg	23	HPMC-AS 1850 mg	Soluplus 1430 mg	90.4	108	114.8
79 FeS SIF	I/P/S	Erlotinib HCl 1000 mg	23	HPMC-AS 1850 mg	Soluplus 1430 mg	259.3	354.8	405.5
80 FaS SIF	I+P+S	Erlotinib HCl (raw) 500 mg	100	HPMC-AS 925 mg	Soluplus 715 mg	78.6	216.4	304.6
81 FeS SIF	I+P+S	Erlotinib HCl (raw) 500 mg	100	HPMC-AS 925 mg	Soluplus 715 mg	16.2	55.8	104.7
82 FaS SIF	I/P+S	Erlotinib HCl 500 mg	35	HPMC-AS 925 mg	Soluplus 715 mg	171.6	284.6	334.6
83 FeS SIF	I/P+S	Erlotinib HCl 500 mg	35	HPMC-AS 925 mg	Soluplus 715 mg	168.3	268.7	317.9

Table 12. Erlotinib - concentration of erlotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution in FaSSIF and FeSSIF solution, respectively presented as comparative data.

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilize r (S)	Compare (%) 5 min	Compare (%) 30 min	Compare (%) 90 min
58 & 69	I	Erlotinib HCl (raw) 1000 mg	100	-	-	543	3038	4261
74 & 75	I+P+S	Erlotinib HCl (raw) 1000 mg	100	HPMC-AS 1850 mg	Soluplus 1430 mg	18	24	29
80 & 81	I+P+S	Erlotinib HCl (raw) 500mg	100	HPMC-AS 925 mg	Soluplus 715 mg	21	26	34
64 & 71	I/P	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	-	310	505	1037
76 & 77	I/P+S	Erlotinib HCl 1000 mg	35	HPMC-AS 1850 mg	Soluplus 1430 mg	106	108	108
82 & 83	I/P+S	Erlotinib HCl 500 mg	35	HPMC-AS 925 mg	Soluplus 715 mg	98	94	95
78 & 79	I/P/S	Erlotinib HCl 1000 mg	23	HPMC-AS 1850 mg	Soluplus 1430 mg	287	329	353

The experiments show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles with erlotinib HCl and a polymeric stabilizing and matrix-forming component. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component hydroxypropyl methylcellulose acetate succinate (HPMC-AS). Experiments 65-66 and 72 show that a further solubility increase is obtained with stable, amorphous hybrid nanoparticles with erlotinib HCl and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added. Particular improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is selected from polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus) and d- α -tocopherol acid polyethylene glycol 1000 succinate (TPGS). This improvement was not observed when the solubilizer was incorporated into the stable, amorphous hybrid nanoparticles.

Physical mixes of erlotinib HCl with a solubilizer and/or HPMC AS improve also the solubility in FaSSIF (experiments 59, 60-61, 62-63) but not in FeSSIF (experiment 69-72). One issue with PKI formulation is the food effect. Several of the PKIs are labeled for administration in fasted state despite the fact that food in most cases increases their bioavailability. Low bioavailability might partly explain the digestive problems that are associated with the PKIs. The data indicates that the stable, amorphous hybrid nanoparticles may reduce food effect and patient digestive problems by its equal solubility improvement in both FaSSIF and FeSSIF (experiment 76/77 and 82/83) that moreover potentially may allow reducing of dosage. Thus, compositions comprising these stable, amorphous hybrid nanoparticles may be given in conjunction with food intake.

Example 3. Compositions with stable, amorphous hybrid nanoparticles with pazopanib – solubility at pH 6.5 and pH 5.

A number of experiments were carried out, wherein pazopanib represented the PKI. The experiments were carried out by measuring concentration of

PKI (mg/L) after 5, 30 and 90 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Further, experiments were carried out in an alternative solution at about pH 5, namely FeSSIF (Fed State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 13 and 14, where Table 13 provides data of concentration of pazopanib (mg/L) after 5, 30 and 90 minutes dissolution, whereas Table 14 provides data of % solubilized pazopanib after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles, compared to pazopanib in raw, crystalline form added to the solution (experiments 84-93). In Tables 15 and 16, there is provided dissolution data in FeSSIF solution, presented similarly as Table 13 and 14 (experiments 94-101). In Table 17, data from a comparative experiment with similar stable, amorphous hybrid nanoparticles, carried out in FaSSIF and FeSSIF, respectively (experiments 102-109). Table 18 presents further comparative data for experiments carried out in FaSSIF and FeSSIF, respectively, with stable, amorphous hybrid nanoparticles.

Table 13. Pazopanib - concentration of pazopanib (mg/L) after 5, 30 and 90 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
84	I	Pazopanib (raw) 1000 mg	100	-	-	46.2	24.4	15.0
85	I+P	Pazopanib (raw) 1000 mg	100	PVP 90K 2000 mg	-	82.7	83.8	67.7
86	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 357 mg	116.3	177.7	204.3
87	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 715 mg	177.6	270.8	324.2
88	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 715 mg	198.8	312.2	394.1
89	I+P+S	Pazopanib (raw)	100	PVP 90K	TPGS	182.6	196.7	49.2

		1000 mg		1857 mg	1000 mg			
90	I/P	Pazopanib 1000 mg	35	PVP 90K 1857 mg	-	89.4	103.4	92.8
91	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 715 mg	238.9	409.4	469.3
92	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	TPGS 1000 mg	207.5	244.8	76.3
93	I/P/S	Pazopanib 1000 mg	28	PVP 90K 1857 mg	Soluplus 715 mg	127.2	128.3	82.0

Table 14. Percentage solubilized pazopanib after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles,

5 compared to pazopanib in raw, crystalline form added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
84	I	Pazopanib (raw) 1000 mg	100	-	-	2.4	2180	-
85	I+P	Pazopanib (raw) 1000 mg	100	PVP 90K 2000 mg	-	8.4	6833	3.1
86	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 357 mg	17.8	15426	7.1
87	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 715 mg	27.1	23899	11.0
88	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 715 mg	31.2	28074	12.9
89	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	TPGS 1000 mg	19.7	12575	5.8
90	I/P	Pazopanib 1000 mg	35	PVP 90K 1857 mg	-	10.3	8520	3.9
91	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 715 mg	40.9	35062	16.1
92	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	TPGS 1000 mg	24.5	15806	7.3
93	I/P/S	Pazopanib 1000 mg	28	PVP 90K 1857 mg	Soluplus 715 mg	12.8	9821	4.5

Table 15. Pazopanib - concentration of pazopanib (mg/L) after 5, 30 and 90 minutes dissolution in FeSSIF solution (pH 5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
94	I	Pazopanib (raw) 1000 mg	100	-	-	231.3	321.4	239.3
95	I+P	Pazopanib (raw) 1000 mg	100	PVP 90K 2000 mg	-	234.8	309.7	269.7
96	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 357 mg	209.3	309.6	229.1

97	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 715 mg	307.5	475.3	578.0
98	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	TPGS 1000 mg	320.9	395.1	325.6
99	I/P	Pazopanib 1000 mg	35	PVP 90K 1857 mg	-	348.4	362.1	335.8
100	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 715 mg	450.0	684.4	777.6
101	I/P/S	Pazopanib 1000 mg	28	PVP 90K 1857 mg	Soluplus 715 mg	226.1	347.3	361.0

Table 16. Percentage solubilized pazopanib after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles, compared to pazopanib in raw, crystalline form added to the FeSSIF solution (pH 5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
94	I	Pazopanib (raw) 1000 mg	100	-	-	32.1	24308	-
95	I+P	Pazopanib (raw) 1000 mg	100	PVP 90K 2000 mg	-	31.0	24775	1.0
96	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 357 mg	31.0	23171	1.0
97	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 715 mg	47.5	42153	1.7
98	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	TPGS 1000 mg	39.5	31373	1.3
99	I/P	Pazopanib 1000 mg	35	PVP 90K 1857 mg	-	36.2	30689	1.3
100	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 715 mg	68.4	59165	2.4
101	I/P/S	Pazopanib 1000 mg	28	PVP 90K 1857 mg	Soluplus 715 mg	34.7	28982	1.2

Table 17. Pazopanib - concentration of pazopanib after 5, 30 and 90 minutes dissolution in FaSSIF and FeSSIF solution, respectively.

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
102 FaSSI F	I+P+S	Pazopanib (raw) 300 mg	100	PVP 90K 557 mg	Soluplus 428 mg	76.8	113.8	139.6
103 FeSSI F	I+P+S	Pazopanib (raw) 300 mg	100	PVP 90K 557 mg	Soluplus 428 mg	116.7	193.6	246.9

104 FaSSI F	I/P+S	Pazopanib 300 mg	35	PVP 90K 557 mg	Soluplus 428 mg	154.7	214.7	223
105 FeSSI F	I/P+S	Pazopanib 300 mg	35	PVP 90K 557 mg	Soluplus 428 mg	186	273.3	303.1
106 FaSSI F	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 1428 mg	261.1	421.6	508.5
107 FeSSI F	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 1428 mg	275.8	495.4	588.0
108F eSSI F	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 1428 mg	508.9	705.8	758.4
109 FeSSI F	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 1428 mg	469.1	715.2	747.4

Table 18. Pazopanib - concentration of pazopanib (mg/L) after 5, 30 and 90 minutes dissolution in FaSSIF and FeSSIF solution, respectively presented as comparative data.

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilize r (S)	Compare (%) 5 min	Compare (%) 30 min	Compare (%) 90 min
84 & 94	I	Pazopanib (raw) 1000 mg	100	-	-	501	1317	1595
85 & 95	I+P	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	-	284	370	398
87 & 96	I+S	Pazopanib (raw) 1000 mg	100	-	Soluplus 715 mg	118	114	71
88 & 97	I+P+S	Pazopanib (raw) 1000 mg	100	PVP 90K 1857 mg	Soluplus 715 mg	155	152	147
102 & 103	I+P+S	Pazopanib (raw) 300 mg	100	PVP 90K 557 mg	Soluplus 428 mg	152	170	177
90 & 99	I/P	Pazopanib 1000 mg	35	PVP 90K 1857 mg	-	390	350	362
89 & 100	I/P+S	Pazopanib 1000 mg	35	PVP 90K 1857 mg	Soluplus 715 mg	188	167	166
104 & 105	I/P+S	Pazopanib 300 mg	35	PVP 90K 557 mg	Soluplus 428 mg	120	127	136
93 & 101	I/P/S	Pazopanib 1000 mg	28	PVP 90K 1857 mg	Soluplus 715 mg	178	271	440

5

Conclusions Example 3

The experiments show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles with

pazopanib and a polymeric stabilizing and matrix-forming component.

Particular improvements are achieved with the polymeric stabilizing and matrix-forming component polyvinylpyrrolidone K-90 (PVP 90K).

Experiments 91-92 show that a further solubility increase is obtained with

5 stable, amorphous hybrid nanoparticles with pazopanib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added. Particular improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is selected from polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus)
10 and d- α -tocopherol acid polyethylene glycol 1000 succinate (TPGS). This improvement was not observed when the solubilizer was incorporated into the stable, amorphous hybrid nanoparticles of the invention.

The results carried out in FaSSIF and FeSSIF, respectively, indicates that
15 the stable, amorphous hybrid nanoparticles of the invention provide a similar increase in solubility. One issue with PKI formulation is the food effect. Several of the PKIs are labeled for administration in fasted state despite the fact that food in most cases increases their bioavailability. Low bioavailability might partly explain the digestive problems that are
20 associated with the PKIs. The similar dissolution rate in FaSSIF and FeSSIF indicates that the stable, amorphous hybrid nanoparticles may reduce food effect and patient digestive problems by its equal solubility improvement in both FaSSIF and FeSSIF (experiments 89/100 and 104/105) that moreover allows reducing dosage. Thus stable, amorphous
25 hybrid nanoparticles of the invention may be given in conjunction with food intake.

Example 4. Compositions with stable, amorphous hybrid nanoparticles with lapatinib – solubility at pH 6.5.

30 A number of experiments were carried out, wherein lapatinib base or lapatinib ditosylate salt represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 5, 30 and 90 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State

Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

- 5 Representative results in FaSSIF solution are provided below in Table 19 and 20, where Table 19 provides data of concentration of lapatinib (mg/L) after 5, 30 and 90 minutes dissolution, whereas Table 20 provides data of % solubilized lapatinib after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC
- 10 increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated lapatinib ditosylate salt added to the solution (experiments 110-126).

Table 19. Lapatinib - concentration of lapatinib (mg/L) after 5, 30 and 90
15 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 5 min	Conc (mg/L) 30 min	Conc (mg/L) 90 min
110	I	Lapatinib (base) 2000 mg	100	-	-	2.9	6.0	6.5
111	I	Lapatinib (salt) 2000 mg	100	-	-	57.7	132.2	124.2
112	I+S	Lapatinib (salt) 2000 mg	100	-	Soluplus 285 mg	67.6	142.9	140.0
113	I+S	Lapatinib (salt) 2000 mg	100	-	Soluplus 645 mg	144.7	283.6	204.0
114	I+P	Lapatinib (base) 2000 mg	100	HPC LF 4000 mg	-	1.9	4.9	6.1
115	I+P	Lapatinib (salt) 2000 mg	100	HPC LF 4000 mg	-	56.7	93.8	81.8
116	I+P+S	Lapatinib (base) 660 mg	100	HPC LF 340 mg	Soluplus 715 mg	5.5	22.5	52.0
117	I+P+S	Lapatinib (salt) 660 mg	100	HPC LF 340 mg	Soluplus 715 mg	71.7	182.5	240.4
118	I+P+S	Lapatinib (base) 660 mg	100	HPC LF 340 mg	TPGS 1000 mg	11.8	40.6	82.9
119	I+P+S	Lapatinib (salt) 660 mg	100	HPC LF 340 mg	TPGS 1000 mg	65.1	176.7	175.3
120	I/P	Lapatinib (base) 660 mg	66	HPC EF 340 mg	-	162.5	184.0	157.1
121	I/P	Lapatinib (base) 660 mg	66	HPC LF 340 mg	-	190.9	193.5	48.0
122	I/P+S	Lapatinib (base) 660 mg	66	HPC EF 340 mg	Soluplus 715 mg	220.4	259.6	280.0
123	I/P+S	Lapatinib (base)	66	HPC LF	Soluplus	200.7	315.6	327.6

		660 mg		340 mg	715 mg			
124	I/P+S	Lapatinib (base) 660 mg	66	HPC EF 340 mg	TPGS 500 mg	202.2	237.5	242.5
125	I/P+S	Lapatinib (base) 660 mg	66	HPC LF 340 mg	TPGS 500 mg	288.4	327.3	301.5
126	I/P/S	Lapatinib (base) 660 mg	66	HPC LF 340 mg	Soluplus 715 mg	57.6	107.2	126.3

Table 20. Percentage solubilized lapatinib after 30 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 90 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated lapatinib ditosylate salt added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 30 min.	AUC/ 90 min Mg/min/L	AUC increase
110	I	Lapatinib (base) 2000 mg	100	-	-	0.3	494	-
111	I	Lapatinib (salt) 2000 mg	100	-	-	6.6	10210	-
112	I+S	Lapatinib (salt) 2000 mg	100	-	Soluplus 285 mg	7.1	11287	1.1
113	I+S	Lapatinib (salt) 2000 mg	100	-	Soluplus 645 mg	14.2	20344	2.0
114	I+P	Lapatinib (base) 2000 mg	100	HPC LF 4000 mg	-	0.2	420	0.04
115	I+P	Lapatinib (salt) 2000 mg	100	HPC LF 4000 mg	-	4.7	7291	0.7
116	I+P+S	Lapatinib (base) 660 mg	100	HPC LF 340 mg	Soluplus 715 mg	3.4	2599	0.3
117	I+P+S	Lapatinib (salt) 660 mg	100	HPC LF 340 mg	Soluplus 715 mg	27.7	16044	1.6
118	I+P+S	Lapatinib (base) 660 mg	100	HPC LF 340 mg	TPGS 1000 mg	6.2	4390	0.4
119	I+P+S	Lapatinib (salt) 660 mg	100	HPC LF 340 mg	TPGS 1000 mg	26.8	13745	1.3
120	I/P	Lapatinib (base) 660 mg	66	HPC EF 340 mg	-	27.9	14971	1.5
121	I/P	Lapatinib (base) 660 mg	66	HPC LF 340 mg	-	29.3	12527	1.2
122	I/P+S	Lapatinib (base) 660 mg	66	HPC EF 340 mg	Soluplus 715 mg	39.3	22739	2.2
123	I/P+S	Lapatinib (base) 660 mg	66	HPC LF 340 mg	Soluplus 715 mg	47.8	26252	2.6
124	I/P+S	Lapatinib (base) 660 mg	66	HPC EF 340 mg	TPGS 500 mg	36.0	20402	2.0
125	I/P+S	Lapatinib (base) 660 mg	66	HPC LF 340 mg	TPGS 500 mg	49.6	27281	2.7
126	I/P/S	Lapatinib (base) 660 mg	66	HPC LF 340 mg	Soluplus 715 mg	16.2	9209	0.9

Conclusions Example 4

The experiments 122-125 clearly shows that a solubility increase is obtained with stable, amorphous hybrid nanoparticles of the invention, with lapatinib, in particular lapatinib base and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component hydroxypropyl cellulose EF and hydroxypropyl cellulose LF. Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is selected from polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus) and d- α -tocopherol acid polyethylene glycol 1000 succinate (TPGS).

Example 5. Compositions with stable, amorphous hybrid nanoparticles with nilotinib HCl – solubility at pH 1.4

A number of experiments were carried out, wherein nilotinib HCl represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 5, 30 and 90 minutes dissolution in a solution at about pH 1.4, namely SGF (Simulated Gastric Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in SGF solution are provided below in Table 21, which provides percentage of solubilized nilotinib HCl from both a physical mix with nilotinib HCl in raw, crystalline form and stable, amorphous hybrid nanoparticles of the invention after 5, 30 and 90 minutes dissolution. Nilotinib present in the physical mix of nilotinib HCl raw with the polymeric stabilizing and matrix-forming component PVAP and the solubilizer Soluplus (Exp. 129) is dissolved completely within 5 minutes in SGF while nilotinib is only partially dissolved after 90 min in SGF with stable, amorphous hybrid nanoparticles of the invention, wherein the components are comprised as stable, amorphous hybrid nanoparticles, with the addition of a solubilizer (Exp. 128) or without the addition of a solubilizer (Exp. 127).

Table 21. Nilotinib HCl - concentration of nilotinib HCl (mg/L) after 5, 30 and 90 minutes dissolution in SGF solution (pH 1.4).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 5 min	% solubilized 30 min	% solubilized 90 min
127	I/P	Nilotinib HCl 500 mg	100	PVAP 750 mg	-	32	40	42
128	I/P+S	Nilotinib HCl 500 mg	100	PVAP 750 mg	Soluplus 715 mg	38	48	50
129	I+P+S	Nilotinib HCl (raw) 1000 mg	100	PVAP 750 mg	Soluplus 715 mg	100	100	100

5 Conclusions Example 5

The experiments 127-129 shows that a nilotinib HCl, in stable, amorphous hybrid nanoparticles of the invention (exp 127 and 128) are partially solubilized at pH 1.4. The stable, amorphous hybrid nanoparticles with a polymeric stabilizing and matrix-forming component such as PVAP is partially protected from the acidic environment.

Example 6. Compositions with stable, amorphous hybrid nanoparticles with gefitinib – solubility at pH 6.5.

A number of experiments were carried out, wherein gefitinib represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 22 and 23, where Table 22 provides data of concentration of gefitinib (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 23 provides data of % solubilized gefitinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention,

compared to non-formulated gefitinib added to the solution (experiments 131-137).

Table 22. Gefitinib - concentration of gefitinib (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 3 min	Conc (mg/L) 40 min	Conc (mg/L) 80 min
131	I	Gefitinib (raw) 1000 mg	100	-	-	121.8	153.1	148.1
132	I+P+S	Gefitinib (raw) 1000 mg	35	PVP30K 1850 mg	Soluplus 715 mg	63.6	158.3	191.1
133	I+P+S	Gefitinib (raw) 1000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	70.6	230.3	296.4
134	I/P	Gefitinib 1000 mg	35	PVP30K 1850 mg	-	501.2	267.2	250.9
135	I/P	Gefitinib 1000 mg	35	HPMCP HP55 1850 mg	-	254.1	321.4	332.1
136	I/P+S	Gefitinib 1000 mg	35	PVP30K 1850 mg	Soluplus 715 mg	561.4	430.2	410.9
137	I/P+S	Gefitinib 1000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	319.8	576.3	594.2

Table 23. Percentage solubilized gefitinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated gefitinib added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 40 min.	AUC/ 80 min Mg/min/L	AUC increase
131	I	Gefitinib (raw) 1000 mg	100	-	-	15.3	5967	-
132	I+P+S	Gefitinib (raw) 1000 mg	35	PVP30K 1850 mg	Soluplus 715 mg	15.8	6630	1.1
133	I+P+S	Gefitinib (raw) 1000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	23.0	9826	1.6
134	I/P	Gefitinib 1000 mg	35	PVP30K 1850 mg	-	26.7	10954	1.8
135	I/P	Gefitinib 1000 mg	35	HPMCP HP55 1850 mg	-	32.1	12794	2.1
136	I/P+S	Gefitinib 1000 mg	35	PVP30K 1850 mg	Soluplus 715 mg	43.0	12282	2.9
137	I/P+S	Gefitinib 1000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	57.6	22774	3.8

The experiments 131-137 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles of the invention, with gefitinib, in particular gefitinib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component polyvinylpyrrolidone K-30 (PVP 30K) and hydroxy propyl methyl cellulose phthalate (HPMCP HP55). Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus).

Example 7. Compositions with stable, amorphous hybrid nanoparticles with dasatinib – solubility at pH 6.5.

A number of experiments were carried out, wherein dasatinib represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 24 and 25, where Table 24 provides data of concentration of dasatinib (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 25 provides data of % solubilized dasatinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated dasatinib added to the solution (experiments 138-141).

Table 24. Dasatinib - concentration of dasatinib (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load	Polymeric stab. matrix.	Solubilizer (S)	Conc (mg/L)	Conc (mg/L)	Conc (mg/L)
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			ratio (%)	Component (P)		3 min	40 min	80 min
138	I	Dasatinib (raw) 1000 mg	100	-	-	34.5	59.7	63.5
139	I+P+S	Dasatinib (raw) 1000 mg	35	Kollidon VA64 1850 mg	Soluplus 715 mg	24.2	64.9	82.5
140	I/P	Dasatinib 1000 mg	35	Kollidon VA64 1850 mg	-	54.7	382.0	417.6
141	I/P+S	Dasatinib 1000 mg	35	Kollidon VA64 1850 mg	Soluplus 715 mg	199.9	599.8	643.8

Table 25. Percentage solubilized dasatinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated dasatinib added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 40 min.	AUC/ 80 min Mg/min/L	AUC increase
138	I	Dasatinib (raw) 1000 mg	100	-	-	6.0	2396	-
139	I+P+S	Dasatinib (raw) 1000 mg	35	Kollidon VA64 1850 mg	Soluplus 715 mg	6.5	2750	1.1
140	I/P	Dasatinib 1000 mg	35	Kollidon VA64 1850 mg	-	35.3	15252	6.4
141	I/P+S	Dasatinib 1000 mg	35	Kollidon VA64 1850 mg	Soluplus 715 mg	58.6	24156	10.1

Experiments 138-141 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles of the invention, with dasatinib, in particular dasatinib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component copolyvidone (Kollidon VA64). Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus).

Example 8. Compositions with stable, amorphous hybrid nanoparticles with Sorafenib tosylate – solubility at pH 6.5.

A number of experiments were carried out, wherein sorafenib tosylate represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 26 and 27, where Table 26 provides data of concentration of sorafenib (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 27 provides data of % solubilized sorafenib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase of compositions, compared to non-formulated sorafenib tosylate added to the solution (experiments 142-145).

Table 26. Sorafenib tosylate - concentration of sorafenib (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 3 min	Conc (mg/L) 40 min	Conc (mg/L) 80 min
142	I	Sorafenib tosylate (raw) 1000 mg	100	-	-	59.1	343.5	311.5
143	I+P+S	Sorafenib tosylate (raw) 1000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	33.9	297.1	352.2
144	I/P	Sorafenib tosylate 1000 mg	35	HPMCP HP55 1850 mg	-	245.3	520.3	613.8
145	I/P+S	Sorafenib tosylate 2000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	335.1	1202.6	1738.1

Table 27. Percentage solubilized sorafenib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated sorafenib tosylate added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solub- ilized 40 min.	AUC/ 80 min Mg/min/L	AUC increase
142	I	Sorafenib tosylate (raw) 1000 mg	100	-	-	34.4	12001	-
143	I+P+S	Sorafenib tosylate (raw) 1000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	33.9	11588	1.0
144	I/P	Sorafenib tosylate 1000 mg	35	HPMCP HP55 1850 mg	-	245.3	21838	1.8
145	I/P+S	Sorafenib tosylate 2000 mg	35	HPMCP HP55 1850 mg	Soluplus 715 mg	335.1	52948	4.4

Experiments 138-141 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles of the invention, with dasatinib, in particular dasatinib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component hydroxy propyl methyl cellulose phthalate (HPMCP HP55). Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus).

Example 9. Compositions with stable, amorphous hybrid nanoparticles with nilotinib base – solubility at pH 6.5.

A number of experiments were carried out, wherein nilotinib base represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 28 and 29, where Table 28 provides data of concentration of nilotinib base (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 29 provides

data of % solubilized nilotinib base after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase of compositions, compared to non-formulated nilotinib base added to the solution (experiments 146-149).

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Table 28. Nilotinib base - concentration of nilotinib base (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 3 min	Conc (mg/L) 40 min	Conc (mg/L) 80 min
146	I/P	Nilotinib base 500 mg	40	HPMCP HP55 750 mg	-	12.7	5.3	3.7
147	I/P	Nilotinib base 500 mg	40	PVAP 750 mg	-	12.3	8.6	7.0
148	I/P+S	Nilotinib base 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	136.8	88.8	41.2
149	I/P+S	Nilotinib base 500 mg	40	PVAP 750 mg	Soluplus 715 mg	20.7	115.9	60.4

Table 29. Percentage solubilized nilotinib base after 40 minutes

dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated nilotinib base added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 40 min.	AUC/ 80 min Mg/min/L	AUC increase
146	I/P	Nilotinib base 500 mg	40	HPMCP HP55 750 mg	-	1.1	242	8.3
147	I/P	Nilotinib base 500 mg	40	PVAP 750 mg	-	1.7	328	11.2
148	I/P+S	Nilotinib base 500 mg	40	HPMCP HP55 750 mg	Soluplus 715 mg	17.8	3529	120.9
149	I/P+S	Nilotinib base 500 mg	40	PVAP 750 mg	Soluplus 715 mg	23.2	3544	121.4

15 **Example 10. Compositions with stable, amorphous hybrid nanoparticles with crizotinib – solubility at pH 6.5.**

A number of experiments were carried out, wherein crizotinib represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH

6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above. Representative results in FaSSIF solution are provided below in Table 30 and 31, where Table 30 provides data of concentration of crizotinib (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 31 provides data of % solubilized crizotinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated crizotinib added to the solution (experiments 150-156).

Table 30. Crizotinib - concentration of crizotinib (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 3 min	Conc (mg/L) 40 min	Conc (mg/L) 80 min
150	I	Crizotinib (raw) 1000 mg	100	-	-	89.3	226.5	295.6
151	I+P+S	Crizotinib (raw) 1000 mg	25	PVP30K 3000 mg	Soluplus 715 mg	176.2	368.5	414.6
152	I+P+S	Crizotinib (raw) 1000 mg	25	PVP30K 3000 mg	Cremophor RH40 715 mg	161.2	428.4	497.7
153	I/P	Crizotinib 1000 mg	25	PVP30K 3000 mg	-	325.9	390.4	398.8
154	I/P	Crizotinib 1000 mg	25	Kollidon VA64 3000 mg	-	297.5	447.6	449.9
155	I/P+S	Crizotinib 1000 mg	25	PVP30K 3000 mg	Soluplus 715 mg	457.6	581.4	578.9
156	I/P+S	Crizotinib 1000 mg	25	PVP30K 3000 mg	Cremophor RH40 715 mg	573.9	855.1	867.2

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Table 31. Percentage solubilized crizotinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated crizotinib added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load	Polymeric stab. matrix.	Solubilizer (S)	% solub- ilized 40	AUC/ 80 min	AUC increase
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			ratio (%)	Component (P)		min.	Mg/min/L	
150	I	Crizotinib (raw) 1000 mg	100	-	-	22.7	16773	
151	I+P+S	Crizotinib (raw) 1000 mg	25	PVP30K 3000 mg	Soluplus 715 mg	36.8	27185	1.6
152	I+P+S	Crizotinib (raw) 1000 mg	25	PVP30K 3000 mg	Cremophor RH40 715 mg	42.8	30423	1.8
153	I/P	Crizotinib 1000 mg	25	PVP30K 3000 mg	-	39.1	29958	1.8
154	I/P	Crizotinib 1000 mg	25	Kollidon VA64 3000 mg	-	44.8	33611	2.0
155	I/P+S	Crizotinib 1000 mg	25	PVP30K 3000 mg	Soluplus 715 mg	58.1	44862	2.7
156	I/P+S	Crizotinib 1000 mg	25	PVP30K 3000 mg	Cremophor RH40 715 mg	85.5	64338	3.8

Experiments 150-156 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles of the invention, with crizotinib, in particular crizotinib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component polyvinylpyrrolidone K-30 (PVP 30K) and copolyvidone (Kollidon VA64). Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is selected from polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus) and PEG-40 hydrogenated castor oil (Cremophor RH40).

Example 11. Compositions with stable, amorphous hybrid nanoparticles with axitinib – solubility at pH 6.5.

A number of experiments were carried out, wherein axitinib represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above.

Representative results in FaSSIF solution are provided below in Table 32 and 33, where Table 32 provides data of concentration of axitinib (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 33 provides data of % solubilized axitinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated axitinib added to the solution (experiments 157-163).

10 **Table 32.** Axitinib - concentration of axitinib (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 3 min	Conc (mg/L) 40 min	Conc (mg/L) 80 min
157	I	Axitinib (raw) 500 mg	100	-	-	0.6	0.6	0.6
158	I+P+S	Axitinib (raw) 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	0.2	0.8	4.3
159	I+P+S	Axitinib (raw) 500 mg	25	HPMC AS 1500 mg	Soluplus 715 mg	0.2	3.0	3.1
160	I/P	Axitinib 500 mg	25	Kollidon VA64 1500 mg	-	71.1	25.9	9.1
161	I/P	Axitinib 500 mg	25	HPMC AS 1500 mg	-	17.6	21.0	16.4
162	I/P+S	Axitinib 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	77.6	223.6	266.1
163	I/P+S	Axitinib 500 mg	25	HPMC AS 1500 mg	Soluplus 715 mg	40.3	110.3	129.9

15 **Table 33.** Percentage solubilized axitinib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated axitinib added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solub- ilized 40 min.	AUC/ 80 min Mg/min/L	AUC increase
157	I	Axitinib (raw) 500 mg	100	-	-	0.1	47	
158	I+P+S	Axitinib (raw) 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	0.2	126	2.7
159	I+P+S	Axitinib (raw) 500 mg	25	HPMC AS 1500 mg	Soluplus 715 mg	0.6	193	4.1

160	I/P	Axitinib 500 mg	25	Kollidon VA64 1500 mg	-	5.2	3255	69.0
161	I/P	Axitinib 500 mg	25	HPMC AS 1500 mg	-	4.2	1571	33.0
162	I/P+S	Axitinib 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	44.7	16070	341.0
163	I/P+S	Axitinib 500 mg	25	HPMC AS 1500 mg	Soluplus 715 mg	22.1	7954	169.0

Experiments 157-163 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles of the invention, with axitinib, in particular axitinib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component copolyvidone (Kollidon VA64) and hydroxypropyl methylcellulose acetate succinate (HPMC AS). Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus).

Example 12. Compositions with stable, amorphous hybrid nanoparticles with vemurafenib – solubility at pH 6.5.

A number of experiments were carried out, wherein vemurafenib represented the PKI. The experiments were carried out by measuring concentration of PKI (mg/L) after 3, 40 and 80 minutes dissolution in a solution at about pH 6.5, namely FaSSIF (Fasted State Simulated Intestinal Fluid). Samples of the solution were taken at various time intervals and the amount of PKI was measured by the dissolution measurement assay described above

Representative results in FaSSIF solution are provided below in Table 34 and 35, where Table 34 provides data of concentration of vemurafenib (mg/L) after 3, 40 and 80 minutes dissolution, whereas Table 35 provides data of % solubilized vemurafenib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the

invention, compared to non-formulated vemurafenib added to the solution (experiments 164-170).

Table 34. Vemurafenib - concentration of vemurafenib (mg/L) after 3, 40 and 80 minutes dissolution in FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	Conc (mg/L) 3 min	Conc (mg/L) 40 min	Conc (mg/L) 80 min
164	I	Vemurafenib (raw) 500 mg	100	-	-	0.3	0.3	0.4
165	I+P+S	Vemurafenib (raw) 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	0.2	0.2	0.4
166	I+P+S	Vemurafenib (raw) 500 mg	25	CAP 1500 mg	Soluplus 715 mg	0.1	0.2	0.4
167	I/P	Vemurafenib 500 mg	25	Kollidon VA64 1500 mg	-	35.5	107.6	122.9
168	I/P	Vemurafenib 500 mg	25	CAP 1500 mg	-	75.1	47.5	11.8
169	I/P+S	Vemurafenib 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	27.4	111.3	172.3
170	I/P+S	Vemurafenib 500 mg	25	CAP 1500 mg	Soluplus 715 mg	55.4	105.7	118.9

Table 35. Percentage solubilized vemurafenib after 40 minutes dissolution, the Area Under the Curve (AUC – mg/min/L) during 80 minutes dissolution and the AUC increase with stable, amorphous hybrid nanoparticles of the invention, compared to non-formulated vemurafenib added to the FaSSIF solution (pH 6.5).

Exp	Comp.	Inhibitor (I)	Drug load ratio (%)	Polymeric stab. matrix. Component (P)	Solubilizer (S)	% solubilized 40 min.	AUC/ 80 min Mg/min/L	AUC increase
164	I	Vemurafenib (raw) 500 mg	100	-	-	0.1	27	
165	I+P+S	Vemurafenib (raw) 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	0.1	21	0.8
166	I+P+S	Vemurafenib (raw) 500 mg	25	CAP 1500 mg	Soluplus 715 mg	0.0	18	0.7
167	I/P	Vemurafenib 500 mg	25	Kollidon VA64 1500 mg	-	21.5	7669	288.0
168	I/P	Vemurafenib 500 mg	25	CAP 1500 mg	-	9.5	3761	141.0
169	I/P+S	Vemurafenib 500 mg	25	Kollidon VA64 1500 mg	Soluplus 715 mg	22.3	8564	322.0
170	I/P+S	Vemurafenib 500 mg	25	CAP 1500 mg	Soluplus 715 mg	21.1	7899	297.0

Experiments 164-170 show that a solubility increase is obtained with compositions comprising stable, amorphous hybrid nanoparticles of the invention, with vemurafenib, in particular vemurafenib and a polymeric stabilizing and matrix-forming component, wherein a separate solubilizer is added to the composition. Particular improvements are achieved with the polymeric stabilizing and matrix-forming component copolyvidone (Kollidon VA64) and cellulose acetate phthalate (CAP). Further, improvements are achieved by the addition of a separate solubilizer added, wherein said solubilizer is polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer (Soluplus).

Example 13. Dissolution rate measurement in sink conditions of compositions of the invention

Dissolution measurement in sink conditions of compositions of the invention were measured in a method consisting of adding the wished amount of powder into a flow through cell system (SOTAX, Allschwill, Switzerland), mounting the cell onto its apparatus and then pumping the appropriate medium (typically FaSSIF, FeSSIF, SGF) through the powder. The temperature of the apparatus was set to 37°C. The amount of powder added into the cell depends on drug load of the powder: The exact amount of powder was calculated from results obtained from drug load analysis of the powders.

Typically, 3.5 to 7 mg PKI was added into the flow through cell and a flow rate between 8 and 16 ml medium/min (preferably about 8 ml medium/min) was pumped through the powder. One ml samples of the medium passing through the cell were collected at predetermined times. These samples were analyzed by HPLC (e.g. C18 column Eclipse, 4.6 mm x 15 cm, 1 ml/min, detection 254-400 nm). Samples were taken after 0, 0.5, 1, 1.5, 2, 3, 4, 5, 6, 7, 8, 9, 10, 15, 20, 25, 30, 35 and 40 min from the moment the medium comes out from the flow through cell. The accumulated % solubilized of the amount of active substance added into the flow through

cell was calculated and plotted against time (min). The initial slope ("initial dissolution rate") of the graph was estimated, as measured during 0 to 10 minutes, and taken as the dissolution rate of the material in sink condition at 37°C in the given dissolution medium.

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Each experiment comprises a comparison between the PKI in raw form with compositions comprising stable, amorphous hybrid particles of the invention with the inhibitor and a representative polymeric stabilizing and matrix-forming component.

10

Example 13.1. Dissolution rate measurement in sink conditions of compositions of the invention, comprising nilotinib HCl

In experiments with nilotinib HCl, 4 mg was weighed in the flow through cell (experiment 500) and compared with stable, amorphous hybrid

15 nanoparticles of the invention with nilotinib base and the polymeric stabilizing and matrix-forming component HPMCP HP55 (experiment 501).

The results are depicted in Table 36 below.

Table 36. Nilotinib HCl sink condition in FaSSIF.

	Experiment 500	Experiment 501
Composition type	I	I/P
Inhibitor (I)	nilotinib HCl (raw)	nilotinib base
Polymeric stab. matrix. Component (P)	-	HPMCP HP55
Drug load %	-	40%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	0.13	3.07
0.5	0.33	7.96
1	0.49	12.23
1.5	0.63	15.22
2	0.76	17.91
3	1.02	23.25
4	1.24	28.03
5	1.48	32.70
6	1.71	37.32
7	1.92	42.04
8	2.13	45.78
9	2.34	49.52

10	2.56	52.34
15	3.51	59.66
20	4.31	66.28
25	5.04	70.92
30	5.7	74.38
35	6.4	76.25
40	7.0	80.33
Initial Dissolution Rate		
EXP 500		0.27
EXP 501		6.58
Ratio 501/500		24.0

Experiments 500-501 show that the initial dissolution rate of the stable, amorphous hybrid nanoparticles of the invention, with nilotinib base, is superior to the initial dissolution rate of nilotinib HCl in raw, crystalline form.

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Example 13.2. Dissolution rate measurement in sink conditions of compositions of the invention comprising erlotinib HCl

In experiments with erlotinib HCl, 3.5 mg was weighed in the flow through cell (experiment 510) and compared with stable, amorphous hybrid

10 nanoparticles of the invention with erlotinib HCl and the polymeric stabilizing and matrix-forming component HPMC AS (experiment 511). The results are depicted in Table 37 below.

Table 37. Erlotinib HCl sink condition in FaSSIF.

	Experiment 510	Experiment 511
Composition type	I	I/P
Inhibitor (I)	erlotinib HCl (raw)	erlotinib HCl
Polymeric stab. matrix. Component (P)	-	HPMC AS
Drug load %	-	35%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	0.26	2.3
0.5	0.49	3.9
1	0.63	5.4
1.5	0.71	6.4
2	0.77	7.2
3	0.85	8.5
4	0.91	9.5
5	0.96	10.3

6	1.01	11.1
7	1.06	11.8
8	1.10	12.5
9	1.13	13.1
10	1.17	13.8
20	1.58	19.3
30	1.93	22.0
40	2.24	24.6
Initial Dissolution Rate		
EXP 510		0.303
EXP 511		2.754
Ratio 511/510		9.1

Experiments 510-511 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with erlotinib HCl and the polymeric stabilizing and matrix-forming component HPMC AS, is superior to the initial dissolution rate of erlotinib HCl in raw, crystalline form.

Example 13.3. Dissolution rate measurement in sink conditions of compositions of the invention comprising pazopanib HCl

In experiments with pazopanib HCl, 3.5 mg was weighed in the flow through cell (experiment 520) and compared with stable, amorphous hybrid nanoparticles of the invention with pazopanib HCl and the polymeric stabilizing and matrix-forming component PVP90K (experiment 521). The results are depicted in Table 38 below.

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Table 38. Pazopanib HCl sink condition in FaSSIF.

	Experiment 520	Experiment 521
Composition type	I	I/P
Inhibitor (I)	pazopanib HCl (raw)	pazopanib HCl
Polymeric stab. matrix. Component (P)	-	PVP90K
Drug load %	-	35%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	1.6	1.9
0.5	4.7	4.6
1	7.7	6.8
1.5	9.6	8.8

2	11.2	10.6
3	13.4	15.2
4	14.7	19.7
5	15.4	22.7
6	16.0	26.2
7	16.4	30.1
8	16.9	33.8
9	17.2	38.2
10	17.6	41.7
20	19.2	73.2
30	20.5	91.3
40	21.6	97.1
		Initial Dissolution Rate Dissolution Rate (5-10 min)
EXP 520		
EXP 521		
Ratio 521/520		

Experiments 520-521 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with pazopanib HCl and the polymeric stabilizing and matrix-forming component PVP90K, is superior to the initial dissolution rate of pazopanib HCl in raw, crystalline form.

Example 13.4. Dissolution rate measurement in sink conditions of compositions of the invention comprising lapatinib ditosylate

In experiments with lapatinib ditosylate, 4 mg was weighed in the flow through cell (experiment 530) and compared with stable, amorphous hybrid nanoparticles of the invention with lapatinib base and the polymeric stabilizing and matrix-forming component HPC If (experiment 531). The results are depicted in Table 39 below.

Table 39. Lapatinib ditosylate sink condition in FaSSIF.

	Experiment 530	Experiment 531
Composition type	I	I/P
Inhibitor (I)	Lapatinib ditosylate (raw)	Lapatinib base
Polymeric stab. matrix. Component (P)	-	HPC If
Drug load %	-	66%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%

0	0.032	0.442
0.5	0.088	1.736
1	0.141	3.053
1.5	0.190	4.448
2	0.238	5.771
3	0.332	7.504
4	0.422	8.783
5	0.505	9.736
6	0.582	10.573
7	0.655	11.209
8	0.725	11.732
9	0.790	12.179
10	0.851	12.576
20	1.272	14.128
30	1.607	15.168
40	1.944	15.802
Initial Dissolution Rate		
EXP 530		0.103
EXP 531		2.674
Ratio 531/530		25.9

Experiments 530-531 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with lapatinib base and the polymeric stabilizing and matrix-forming component HPC If, is superior to the initial dissolution rate of lapatinib ditosylate in raw, crystalline form.

Example 13.5. Dissolution rate measurement in sink conditions of compositions of the invention comprising gefitinib

In experiments with gefitinib, 3.5 mg was weighed in the flow through cell (experiment 540) and compared with stable, amorphous hybrid nanoparticles of the invention with gefitinib and the polymeric stabilizing and matrix-forming component HPMCP HP55 (experiment 541). The results are depicted in Table 40 below.

Table 40. Gefitinib sink condition in FaSSIF.

	Experiment 540	Experiment 541
Composition type	I	I/P
Inhibitor (I)	Gefitinib (raw)	Gefitinib
Polymeric stab. matrix. Component	-	HPMCP HP55

(P)		
Drug load %	-	35%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	0.1	1.8
0.5	0.9	6.7
1	1.9	11.3
1.5	3.2	15.4
2	4.5	19.0
3	7.0	23.6
4	9.5	27.4
5	11.9	30.5
6	14.3	33.5
7	16.6	36.0
8	18.8	37.8
9	20.7	39.9
10	22.7	42.6
20	29.9	50.6
30	34.1	56.7
40	36.7	61.8
Initial Dissolution Rate		
EXP 540		2.2
EXP 541		8.6
Ratio 541/540		3.9

Experiments 540-541 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with gefitinib and the polymeric stabilizing and matrix-forming component HPMCP HP55, is superior to the initial dissolution rate of the gefitinib in raw, crystalline form.

Example 13.6. Dissolution rate measurement in sink conditions of compositions of the invention comprising dasatinib

In experiments with dasatinib, 3.5 mg was weighed in the flow through cell (experiment 550) and compared with stable, amorphous hybrid nanoparticles of the invention with dasatinib and the polymeric stabilizing and matrix-forming component copolyvidon - Kollidon VA64 (experiment 551). The results are depicted in Table 41 below.

Table 41. Dasatinib sink condition in FaSSIF.

	Experiment 550	Experiment 551
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Composition type	I	I/P
Inhibitor (I)	Dasatinib (raw)	Dasatinib
Polymeric stab. matrix. Component (P)	-	Kollidon VA64
Drug load %	-	35%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	0.3	0.4
0.5	0.7	1.0
1	1.2	1.7
1.5	1.6	2.3
2	2.0	2.9
3	2.8	4.2
4	3.7	5.5
5	4.4	6.8
6	5.2	8.2
7	6.0	9.5
8	6.8	10.8
9	7.6	12.1
10	8.3	13.4
20	15.9	25.9
30	22.1	40.9
40	26.4	54.9
Initial Dissolution Rate		
EXP 550		0.8
EXP 551		1.3
Ratio 551/550		1.6

Experiments 550-551 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid of the invention, with dasatinib and the polymeric stabilizing and matrix-forming component copolyvidon (Kollidon VA64), is superior to the initial dissolution rate of the dasatinib raw, crystalline form.

Example 13.7. Dissolution rate measurement in sink conditions of compositions the invention comprising sorafenib tosylate

In experiments with sorafenib tosylate, 3.5 mg was weighed in the flow through cell (experiment 560) and compared with stable, amorphous hybrid nanoparticles of the invention with sorafenib tosylate and the polymeric stabilizing and matrix-forming component HPMCP HP55 (experiment 561). The results are depicted in Table 42 below.

Table 42. Sorafenib tosylate sink condition in FaSSiF.

	Experiment 560	Experiment 561
Composition type	I	I/P
Inhibitor (I)	Sorafenib tosylate (raw)	Sorafenib tosylate
Polymeric stab. matrix. Component (P)	-	HPMCP HP55
Drug load %	-	35%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	0.2	0.8
0.5	0.4	1.7
1	0.7	2.4
1.5	1.0	3.1
2	1.3	3.7
3	1.8	4.8
4	2.2	5.8
5	2.6	6.9
6	3.0	8.1
7	3.4	9.7
8	3.8	11.3
9	4.2	13.3
10	4.6	15.6
20	8.8	32.7
30	12.6	61.5
40	16.4	96.1
Initial Dissolution Rate		
EXP 560		0.47
EXP 561		1.17
Ratio 561/560		2.5

Experiments 560-561 show that the initial dissolution rate of the

- 5 compositions comprising stable, amorphous hybrid nanoparticles of the invention, with sorafenib tosylate and the polymeric stabilizing and matrix-forming component HPMCP HP55, is superior to the initial dissolution rate of sorafenib tosylate in raw, crystalline form.

10 **Example 13.8. Dissolution rate measurement in sink conditions of compositions of the invention comprising crizotinib**

In experiments with crizotinib, 3.5 mg was weighed in the flow through cell (experiment 570) and compared with stable, amorphous hybrid

nanoparticles of the invention with crizotinib and the polymeric stabilizing and matrix-forming component PVP 30K (experiment 571). The results are depicted in Table 43 below.

5 Table 43. Crizotinib sink condition in FaSSIF.

	Experiment 570	Experiment 571
Composition type	I	I/P
Inhibitor (I)	Crizotinib (raw)	Crizotinib
Polymeric stab. matrix. Component (P)	-	PVP 30K
Drug load %	-	25%
Accumulated % of solubilized of remaining active substance at a given time (min)		
Min.	%	%
0	2.0	8.8
0.5	5.7	30.3
1	8.9	47.9
1.5	11.9	58.3
2	14.6	67.5
4	23.1	81.7
6	30.1	83.8
8	36.0	84.2
10	41.0	84.4
20	58.9	85.1
30	73.1	85.3
40	86.3	85.5
Initial Dissolution Rate		
EXP 570		6.6
EXP 571		33.3
Ratio 571/570		5.0

Experiments 570-571 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with crizotinib and the polymeric stabilizing and matrix-forming component PVP 30K, is superior to the initial dissolution rate of crizotinib in raw, crystalline form.

Example 13.9. Dissolution rate measurement in sink conditions of compositions of the invention comprising axitinib

15 In experiments with axitinib, 3.5 mg was weighed in the flow through cell (experiment 580) and compared with stable, amorphous hybrid nanoparticles of the invention with axitinib and the polymeric stabilizing

and matrix-forming component Kollidon VA64 (experiment 581) or HPMC AS (experiment 582). The results are depicted in Table 44 below.

Table 44. Axitinib sink condition in FaSSIF.

	Experiment 580	Experiment 581	Experiment 582
Composition type	I	I/P	I/P
Inhibitor (I)	Axitinib (raw)	Axitinib	Axitinib
Polymeric stab. matrix. Component (P)	-	Kollidon VA64	HPMC AS
Drug load %	-	25%	25%
Accumulated % of solubilized of remaining active substance at a given time (min)			
Min.	%	%	%
0	0.03	0.75	0.22
0.5	0.06	1.60	0.59
1	0.08	2.33	1.04
1.5	0.11	2.97	1.50
2	0.13	3.56	1.92
4	0.23	6.03	3.25
6	0.31	7.76	4.39
8	0.40	9.74	5.34
10	0.49	11.81	6.17
20	0.97	22.04	9.03
30	1.46	27.42	11.43
40	1.96	30.53	13.52
Initial Dissolution Rate			
EXP 580		0.051	
EXP 581 & 582		1.396	0.865
Ratio 581/580 & 582/580		27.5	17.1

5

Experiments 580-582 show that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with axitinib and the polymeric stabilizing and matrix-forming component Kollidon VA64 or HPMC AS, is superior to the initial dissolution rate of axitinib in raw, crystalline form.

10

Example 13.10. Dissolution rate measurement in sink conditions of compositions of the invention comprising vemurafenib

In experiments with vemurafenib, 3.5 mg was weighed in the flow through cell (experiment 590) and compared with stable, amorphous hybrid nanoparticles of the invention with vemurafenib and the polymeric

15

stabilizing and matrix-forming component Kollidon VA64 (experiment 591) or CAP (experiment 592). The results are depicted in Table 45 below.

Table 45. Vemurafenib sink condition in FaSSIF.

	Experiment 590	Experiment 591	Experiment 592
Composition type	I	I/P	I/P
Inhibitor (I)	Vemurafenib (raw)	Vemurafenib	Vemurafenib
Polymeric stab. matrix. Component (P)	-	Kollidon VA64	CAP
Drug load %	-	25%	25%
Accumulated % of solubilized of remaining active substance at a given time (min)			
Min.	%	%	%
0	0.0	0.1	0.4
0.5	0.0	0.2	1.1
1	0.0	0.3	1.8
1.5	0.0	0.4	2.4
2	0.0	0.5	3.1
4	0.0	1.2	6.3
6	0.0	1.9	9.4
8	0.0	2.4	11.0
10	0.0	2.9	12.1
20	0.0	4.7	14.9
30	0.1	5.9	16.8
40	0.1	7.1	18.3
Initial Dissolution Rate			
EXP 590		0.002	
EXP 591 & 592		0.209	1.346
Ratio 591/590 & 592/590		104	673

5

Experiments 590-592 clearly shows that the initial dissolution rate of the compositions comprising stable, amorphous hybrid nanoparticles of the invention, with vemurafenib and the polymeric stabilizing and matrix-forming component Kollidon VA64 or CAP, is superior to the initial dissolution rate of vemurafenib in raw, crystalline form.

10

Example 14. *In vivo* measurement of plasma levels after oral administration of compositions of the invention

Groups of four beagle dogs received single oral doses (5 mg/kg) of capsule compositions comprising stable, amorphous hybrid nanoparticles of the invention with nilotinib base and either of the polymeric stabilizing and matrix-forming components PVAP or HPMCP HP55, optionally with

15

addition of the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer, and compared with a marketed formulation comprising nilotinib HCl. The stable, amorphous hybrid nanoparticles tested are as set out in experiments 146-149, in Example 9. The stomach contents of the dogs were either neutralized with a sodium bicarbonate solution 5 min prior to capsule dosing or acidified with an HCl-KCl buffer 10 min prior to dose. One group of dogs also received a single iv dose (1 mg/kg) of nilotinib. Plasma levels of nilotinib were determined with a selective LC-MS/MS method. There were no side-effects observed in any animal studied.

Results and conclusions

Mean $\pm$ SEM plasma concentration-time profiles of nilotinib base are shown in Figures 22-25, and pharmacokinetic parameters and results are displayed in Tables 46A and 46B.

Outliers were calculated and excluded based on if one value is a significant outlier from the rest at 95% confidence intervals ($\alpha = 5\%$) according to Grubb's test. The critical Z value for the Grubb's test at the 95% confidence interval with $n=4$ is 1.48. $Z = (\text{Mean} - \text{Questionable value})/\text{SD}$

Table 46A. Pharmacokinetic data following single oral administration of different nilotinib compositions of the invention, in dogs.

	Marketed nilotinib formulation	Marketed nilotinib formulation	I/P Nilotinib base/ PVAP Exp 147	I/P+S Nilotinib base/ PVAP + Soluplus Exp 149	I/P Nilotinib base/ PVAP Exp 147
	Acidic Stomach	Neutral Stomach	Acidic Stomach	Acidic Stomach	Neutral Stomach
C _{max} , ng/mL	86 $\pm$ 52	73 $\pm$ 26	240 $\pm$ 87	360 $\pm$ 89	490 $\pm$ 350
T _{max} , hr	7.6 $\pm$ 11	1.3 $\pm$ 0.3	1.3 $\pm$ 0.3	1.3 $\pm$ 0.3	1.4 $\pm$ 0.5
T $\frac{1}{2}$, hr	9.9; 10.7	1.9 $\pm$ 0.3	4.3 $\pm$ 3.0	3.3 $\pm$ 2.0	3.4 $\pm$ 1.2
AUC 0-24h, ng*hr/mL	400 $\pm$ 140	220 $\pm$ 90	650 $\pm$ 240	1260 $\pm$ 70	1820 $\pm$ 1200

F (%)	7.9 ± 2.9	4.4 ± 1.8	13 ± 5	25 ± 1	36 ± 24
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Values are given as Mean±SD, except for T_{1/2} of the Marketed nilotinib formulation given too acid stomach where only two values were obtained.

- 5 Intravenous (IV) data were obtained by constant rate IV infusion of 1 mg/kg, of a solution of Nilotinib at 0.2 mg/mL, in a 10% HPβCD, pH adjustment to pH 3.3 to 3.5. Co: 511±46 ng/mL; T_{1/2}: 3.3±1.8 hr; AUC_{0-24hr}: 1000±300 ng*hr/mL
- 10 Table 46B. Pharmacokinetic data following single oral administration of different nilotinib formulations of the invention, in dogs.

	I/P Nilotinib base/ HPMCP HP55 Exp 146	I/P Nilotinib base/ HPMCP HP55 + Soluplus Exp 148	I/P Nilotinib base/ HPMCP HP55 Exp 146	I/P Nilotinib base/ HPMCP HP55 + Soluplus Exp 148
	Neutral Stomach	Neutral Stomach	Acidic Stomach	Acidic Stomach
C _{max} , ng/mL	210 ± 97	560 ± 220	380 ± 90	270 ± 130
T _{max} , hr	1.1 ± 0.5	1.3 ± 0.29	1.2 ± 0.3	1.0 ± 0.0
T _{1/2} , hr	1.9 ± 0.2	3.0 ± 1.4	3.3 ± 1.3	3.8 ± 0.8
AUC 0-24h, ng*hr/mL	730 ± 390	1600 ± 580	1230 ± 110	910 ± 630
F (%)	15 ± 8	32 ± 12	24 ± 2	18 ± 13

Values are given as Mean±SD

- Intravenous (IV) data were obtained by constant rate IV infusion of 1 mg/kg, of a solution of Nilotinib at 0.2 mg/mL, in a 10% HPβCD, pH adjustment to pH 3.3 to 3.5. Co: 511±46 ng/mL; T_{1/2}: 3.3±1.8 hr; AUC_{0-24hr}: 1000±300 ng*hr/mL.
- 15

- The marketed nilotinib formulation administrated to an acidified stomach showed plasma levels about 2 times higher than those after the same formulation administered to a neutralized stomach. Both formulations comprising stable, amorphous hybrid nanoparticles of the invention with nilotinib base with PVAP and HPMCP HP55 as polymeric stabilizing and matrix-forming components showed significant improvements in plasma
- 20

exposure, with plasma levels about 2-fold higher than those of the marketed formulation given to an acidified stomach. In addition, combining stable, amorphous hybrid nanoparticles produced by the methods of the invention could give a plasma exposure that is be more or less
5 independent of stomach pH.

Further improvements in oral availability were observed when formulations with stable, amorphous hybrid nanoparticles of the invention were combined with the solubilizer polyvinyl caprolactam-polyvinyl acetate-
10 polyethylene glycol copolymer. Thus, compositions of the invention with nilotinib base with PVAP and HPMCP HP55 as polymeric stabilizing and matrix-forming components, where the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer was added and administered to an acidified stomach resulted in plasma levels 2.3- to 3.1-
15 fold higher than those of the marketed formulation. In this study, high oral bioavailability was achieved with stable, amorphous hybrid nanoparticles of the invention with nilotinib base with HPMCP HP55 as polymeric stabilizing and matrix-forming components, where the solubilizer polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer was added
20 (I/P+S) and administrated to neutralized stomach contents. In this case the exposure increased about 7-fold over that of the marketed oral formulation administered under the same neutralized conditions. Highest bioavailability, $36\pm24\%$, in this study was achieved when stable, amorphous hybrid nanoparticles of the invention with nilotinib base with PVAP as polymeric
25 stabilizing and matrix-forming component was administered to a neutralized stomach. However, this study leg was also accompanied with the highest standard deviation in the study.

There was an improvement in the *in vivo* performance of the compositions
30 of the present invention with of nilotinib stable, amorphous hybrid nanoparticles, that are based on improving absorption and bioavailability by optimization of the solid state properties of the dosage form. The results

of the *in vivo* study in dogs may predict similar absorption properties of stable, amorphous hybrid nanoparticles of the invention, in patients, as there appears to be a close correlation in dog-human gastrointestinal drug absorption processes (Persson, E.M. et al. Pharm. Res. 2005, 22, 2141-
5 2151). The stable, amorphous hybrid nanoparticles of the invention, with advantageous absorption properties, also predict that the oral doses used in clinical practice today may be lowered. Furthermore, the stable, amorphous hybrid nanoparticles of the invention may cause less pH-dependency in the absorption and bioavailability of PKIs.

10

Example 15. Measurement of degree/level of stability of compositions with hybrid nanoparticles of the invention

In stability tests of compositions comprising hybrid nanoparticles of the invention, it was shown that particles were stable over at least 11 months
15 at room temperature (18-25°C), as measured by X-Ray powder diffraction and dissolution rate by measurement of AUC.

In series of experiments with stable, amorphous hybrid nanoparticles comprising nilotinib and HPMCP HP55 produced by the methods of the
20 invention, the resulting particles provided stable, amorphous hybrid nanoparticles at 40% drug load (I/P nilotinib base/HPMCP HP55: exp 146), as measured by XRPD as well as dissolution rate by measurement of AUC. The material showed one glass transition temperature at ca 127 °C, which indicate a single amorphous phase with inherent stability. Partially
25 crystalline batches also processed similar inherent stability. 6 months storage at room temperature (18-25 °C) of partly crystalline hybrid nanoparticles at 40% drug load, I/P nilotinib base/HPMCP HP55, did not show any signs of physical instability.

30 Thermalgravimetric analysis provided a mass loss of 1.7 % from ambient temperature to 120°C.

Dynamic vapor absorption analysis at 25 °C gave a relative mass increase of ca 7% from 0 to 90% RH (Three cycles from 0 to 90% RH, did not induce a phase change).

- 5 The high glass transition temperature, 1.7% mass loss from ambient temperature to 120°C and moderate hygroscopicity propose an inherent stability. This is supported by stability testing of several batches at various conditions. The longest stability point is 12 months at room temperature (18 – 25°C). No batches or conditions have shown any signs of physical
10 instability (Figure 27).

Modulated Differential Scanning Calorimetry (mDSC)

Modulated Differential Scanning Calorimetry (mDSC) analysis was run on a TA Instruments Model Q200 (New Castle, USA), equipped with a RC90
15 refrigerated cooling system (Home Automation, New Orleans, USA). Samples were weighed to 7±2 mg in Tzero Low-mass aluminum pans and sealed with Tzero lids. They were then heated at a heating rate of 3°C/min from 0 to 170°C with conventional modulation temperature amplitude of 1°C and a modulation period of 40 seconds. Ultra-high purity nitrogen was
20 used as purge gas at a flow rate of 50 mL/min. All data analyses were performed using TA Universal Analysis software, version 4.7A. Cell constant and temperature calibrations were conducted with the use of an indium standard prior to instrument operation. DSC results were evaluated in terms of both forward and reverse components of heat flow.

25

Thermogravimetry (TG) was performed on a Seiko TG/DTA 6200 and open 90 µl Pt-pans with ca 10 to 20 mg of sample and a nitrogen flow of 200 mL/min. The temperature program was ambient (20°C) to 400°C with a heating rate of 10 °C/min. A blank was subtracted and the TG data was
30 normalized with respect to sample size and analyzed using the Muse Standard Analysis software, version 6.1 U.

Dynamic Vapour Sorption (DVS)

The hygroscopicity of the samples was studied by Dynamic Vapor Sorption Gravimetry (DVS), using a DVS-1 (Surface Measurement Ltd., UK).

Approximately 10 mg of the substance was weighed into a glass cup. The
5 relative weight was recorded at 20 second interval when the target relative humidity (RH) over the sample was increased stepwise from 0% to 90%, and then similarly decreased back to 0% RH, with 10% RH per step. Each sample was run in three consecutive full cycles. The condition to proceed to the next level of RH was a weight change below or equal to 0.002%
10 within 15 minutes, with a maximum total time per step of 24 hours. Due to slow equilibration in experiments of this type, the numbers obtained should be regarded as lower estimates of water uptake. The temperature was kept at 25°C.

15 *X-Ray Powder Diffraction (XRPD)*

XRD experiments were run on an X'Pert Pro diffractometer (PANanalytical, Almelo, Netherlands) set in Bragg-Brentano geometry. The diffractometer was equipped with 20 µm nickel filter and an X'Celerator RTMS detector with an active length of $2.122^\circ 2\theta$. A representative
20 sample was placed on a zero background quartz single crystal specimen support (Siltronix, Archamps, France). Experiments were run using Cu K_α radiation (45kV and 40 mA) at ambient temperature and humidity. Scans were run in continuous mode in the range $4.5\text{--}40^\circ 2\theta$ using automatic divergence and anti-scatter slits with observed length of 10 mm, a common
25 counting time of 299.72 seconds, and step size of $0.0167^\circ 2\theta$. Data collection was done using the application software X'Pert Data Collector V.2.2j and instrument control software V.2.1E, while pattern analysis was done using X'Pert Data Viewer V.1.2c (all software being from
PANanalytical, Almelo, Netherlands).

30

Dissolution rate by measurement of AUC

The stable hybrid nanoparticles described in Exp 171 & Exp172 (I/P) as set out below, were produced according to Exp 148, with nilotinib base, HPMCP HP55 and stored at room temperature for 11 months. The non-sink dissolution rate was tested at different different time points and the results are presented in Table 47 and Figure 26. Polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer was added to enhance solubility. A comparison of the AUC over 80 minutes show clearly that the dissolution rate profile of the particles is practically unchanged after 11 months storage, e.g. the ratio between the AUC of particles produced and tested, compared to particles produced, tested and stored for 11 months is over 97%.

Table 47.

	0	1 min	5 min	10 min	20 min	40 min	80 min	AUC	Ratio (%)
Exp 171 (t=0, n=1)	0	70,5	144,8	172,8	155,8	67,7	46,0	7411,9	
Exp 171 (t=11 months, n=3)	0	20,2	110,7	149,5	158,5	83,6	34,0	7234,5	97,6
Standard deviation	0	5,8	14,3	19,6	19,6	3,5	1,5		

Claims

1. A pharmaceutical composition comprising stable, amorphous solid dispersion particles of dasatinib and at least one polymeric stabilizing and matrix-forming component; which composition optionally further comprises at least one pharmaceutically acceptable solubilizer; wherein said dasatinib is present in an amount of from about 10% by weight to about 70% by weight of the amorphous particles; wherein the particles are obtained by mixing i) a pressurized solution comprised of dasatinib and a solvent and ii) a pressurized antisolvent, and wherein said at least one polymeric stabilizing and matrix-forming component is provided in either one or both of the pressurized solution or the pressurized antisolvent.
2. The composition of claim 1, wherein said stable, amorphous solid dispersion particles are stable amorphous hybrid nanoparticles.
3. The composition of claim 1 or claim 2, wherein the amount of dasatinib is from about 10% by weight to about 50% by weight of the amorphous particles.
4. The composition of claim 1 or claim 2, wherein the amount of dasatinib is from about 10% by weight to about 40% by weight of the amorphous particles.
5. The composition of claim 1 or claim 2, wherein the amount of dasatinib is from about 10% by weight to about 30% by weight of the amorphous particles.
6. The composition according to any one of claims 1-5, wherein said dasatinib is dasatinib hydrate, dasatinib solvate, or combinations thereof.
7. The composition according to any one of claims 1-6, wherein the amorphous particles have a degree of amorphicity of 100%.
8. The composition according to any one of claims 1-7, wherein the at least one polymeric stabilizing and matrix-forming component is selected from the group consisting of hydroxypropyl methylcellulose phthalate, hydroxypropyl cellulose, copolyvidone,

hydroxypropyl methylcellulose acetate succinate, polyvinyl acetate phthalate, cellulose acetate phthalate and polyvinylpyrrolidone.

9. The composition according to any one of claims 1-7, wherein the at least one polymeric stabilizing and matrix-forming component is copolyvidone.
10. The composition according to any one of claims 1 to 9, which composition further comprises at least one pharmaceutically acceptable solubilizer.
11. The composition of claim 10, wherein the solubilizer is selected from the group consisting of polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol copolymer, d- α -tocopherol acid polyethylene glycol 1000 succinate, a hydrogenated castor oil, a PEG-35 castor oil, a PEG-40 stearate, a hard fat, a polyoxylglyceride, a PEG-8 caprylic/capric glyceride, and a poloxamer.
12. The composition according to claim 10 or 11 wherein said solubilizer is present separated from the particles in the composition.
13. The composition according to claim 10 or 11, wherein said solubilizer is distributed to the surface of the particles.
14. The composition according to any one of claims 1 to 13, wherein said composition provides an increased dissolution rate, compared to the dissolution rate of said dasatinib in raw, crystalline form.
15. The composition according to any one of claims 1 to 14, which provides a solubility increase of dasatinib in a solution, said increase measured as the area under the curve (AUC) during about from 40 minutes to about 90 minutes, in said solution as compared with the AUC of dasatinib in raw, crystalline form.
16. The composition according to any one of claims 1 to 15, wherein the dissolution rate of said stable, amorphous particles remain stable to at least about 90%, after 9 months of storage or more, at room temperature.

17. The composition according to any one of claims 1 to 16, wherein said stable, amorphous particles has an average particle diameter size of less than about 1000 nm.
18. The composition of claim 17, wherein said particle diameter size is less than about 500 nm.
19. Use of a composition according to any one of claims 1 to 18, in the manufacture of a medicament.
20. Use of a composition according to any one of claims 1 to 18, in the manufacture of a medicament for the treatment of proliferative disorders.
21. The use of a composition in the manufacture of a medicament according to claim 20, wherein said proliferative disorder is selected from tumours and cancers.
22. The use of a composition in the manufacture of a medicament according to claim 20, wherein said proliferative disorder is selected from neurofibromatosis, tuberous sclerosis, hemangiomas and lymphangiogenesis, cervical, anal and oral cancers, eye or ocular cancer, stomach cancer, colon cancer, bladder cancer, rectal cancer, liver cancer, pancreas cancer, lung cancer, breast cancer, cervix uteri cancer, corpus uteri cancer, ovary cancer, prostate cancer, testis cancer, renal cancer, brain cancer, cancer of the central nervous system, head and neck cancer, throat cancer, skin melanoma, acute lymphocytic leukemia, acute myelogenous leukemia, Ewing's Sarcoma, Kaposi's Sarcoma, basal cell carcinoma and squamous cell carcinoma, small cell lung cancer, choriocarcinoma, rhabdomyosarcoma, angiosarcoma, hemangioendothelioma, Wilms Tumor, neuroblastoma, mouth/pharynx cancer, esophageal cancer, larynx cancer, lymphoma, multiple myeloma; cardiac hypertrophy, age-related macular degeneration and diabetic retinopathy.
23. The use of a composition in the manufacture of a medicament according to any one of claims 20 to 22, wherein said medicament is provided during food intake,
24. Use of a composition according to any one of claims 1 to 18 for therapy.

25. Use of a composition according to any one of claims 1 to 18, for the treatment of proliferative disorders.
26. The use according to claim 25, wherein said proliferative disorder is selected from tumours and cancers.
27. The use according to claim 25, wherein said proliferative disorder is selected from neurofibromatosis, tuberous sclerosis, hemangiomas and lymphangiogenesis, cervical, anal and oral cancers, eye or ocular cancer, stomach cancer, colon cancer, bladder cancer, rectal cancer, liver cancer, pancreas cancer, lung cancer, breast cancer, cervix uteri cancer, corpus uteri cancer, ovary cancer, prostate cancer, testis cancer, renal cancer, brain cancer, cancer of the central nervous system, head and neck cancer, throat cancer, skin melanoma, acute lymphocytic leukemia, acute myelogenous leukemia, Ewing's Sarcoma, Kaposi's Sarcoma, basal cell carcinoma and squamous cell carcinoma, small cell lung cancer, choriocarcinoma, rhabdomyosarcoma, angiosarcoma, hemangioendothelioma, Wilms Tumor, neuroblastoma, mouth/pharynx cancer, esophageal cancer, larynx cancer, lymphoma, multiple myeloma; cardiac hypertrophy, age-related macular degeneration and diabetic retinopathy.
28. The use according to any one of claims 25 to 27, wherein said composition is provided during food intake.
29. A method of providing therapy comprising administering to a patient in need thereof a composition according to any one of claims 1 to 18.
30. A method of treating proliferative disorders comprising administering to a patient in need thereof a composition according to any one of claims 1 to 18.
31. The method according to claim 30, wherein said proliferative disorder is selected from tumours and cancers.
32. The method according to claim 30, wherein said proliferative disorder is selected from neurofibromatosis, tuberous sclerosis, hemangiomas and lymphangiogenesis, cervical, anal and oral cancers, eye or ocular cancer, stomach cancer, colon cancer, bladder

cancer, rectal cancer, liver cancer, pancreas cancer, lung cancer, breast cancer, cervix uteri cancer, corpus uteri cancer, ovary cancer, prostate cancer, testis cancer, renal cancer, brain cancer, cancer of the central nervous system, head and neck cancer, throat cancer, skin melanoma, acute lymphocytic leukemia, acute myelogenous leukemia, Ewing's Sarcoma, Kaposi's Sarcoma, basal cell carcinoma and squamous cell carcinoma, small cell lung cancer, choriocarcinoma, rhabdomyosarcoma, angiosarcoma, hemangioendothelioma, Wilms Tumor, neuroblastoma, mouth/pharynx cancer, esophageal cancer, larynx cancer, lymphoma, multiple myeloma; cardiac hypertrophy, age-related macular degeneration and diabetic retinopathy.

33. The method according to any one of claims 29 to 32, wherein said composition is provided during food intake.

Figure 1

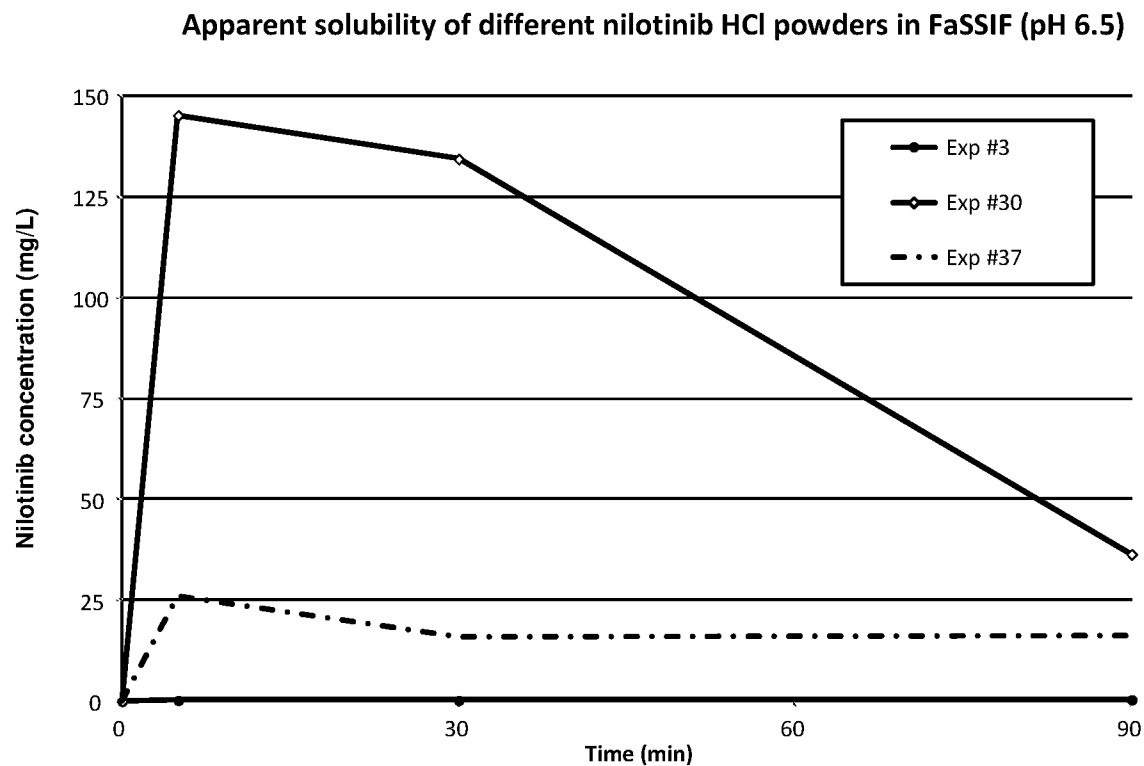


Figure 2

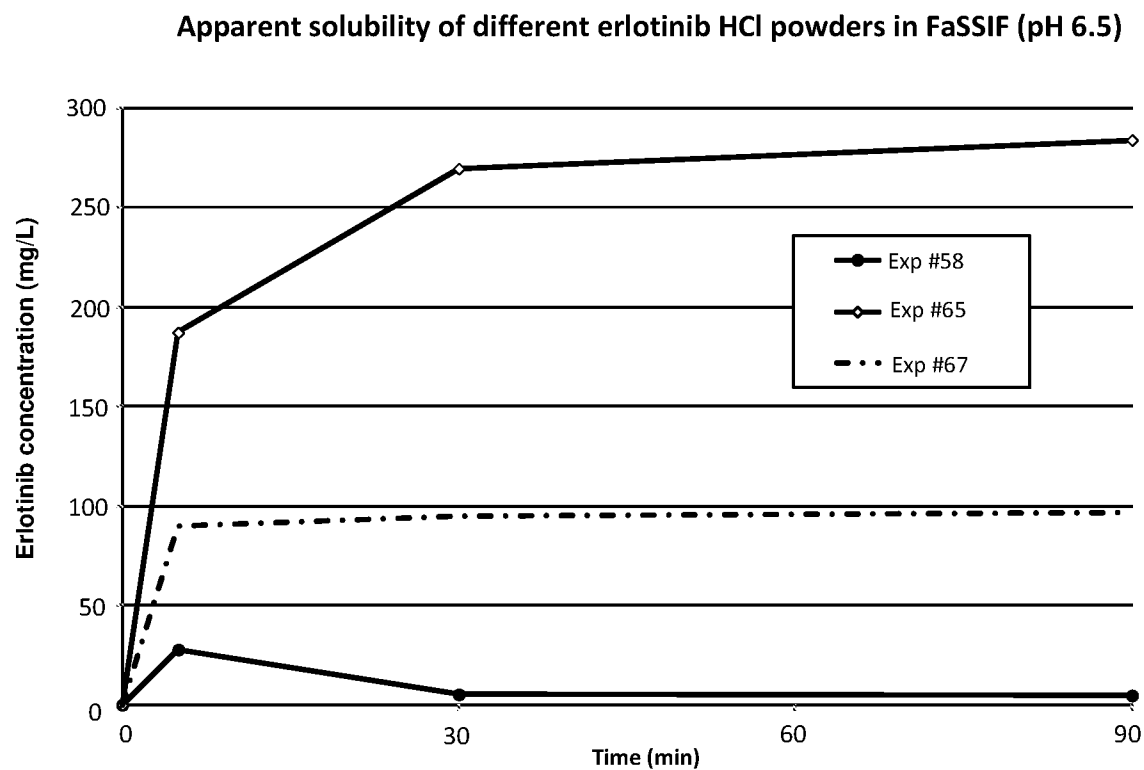


Figure 3

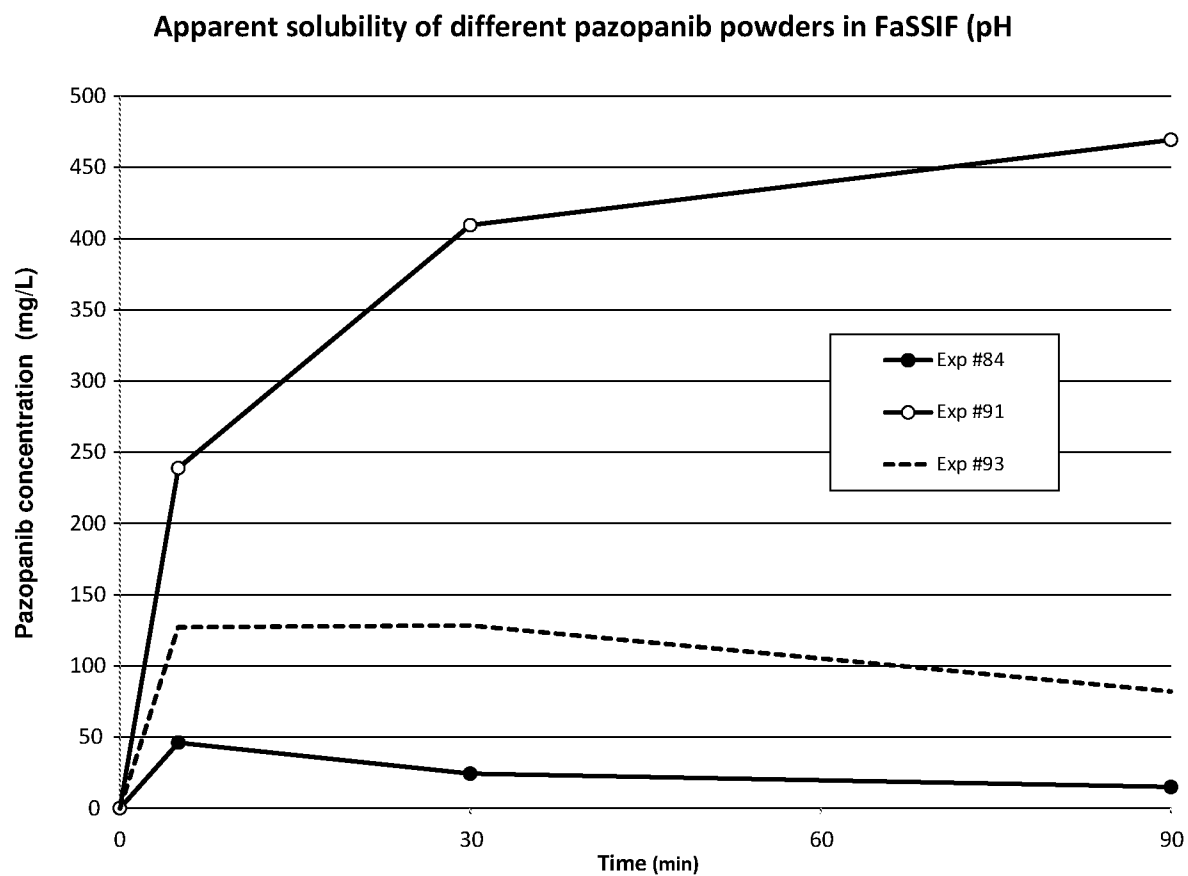


Figure 4

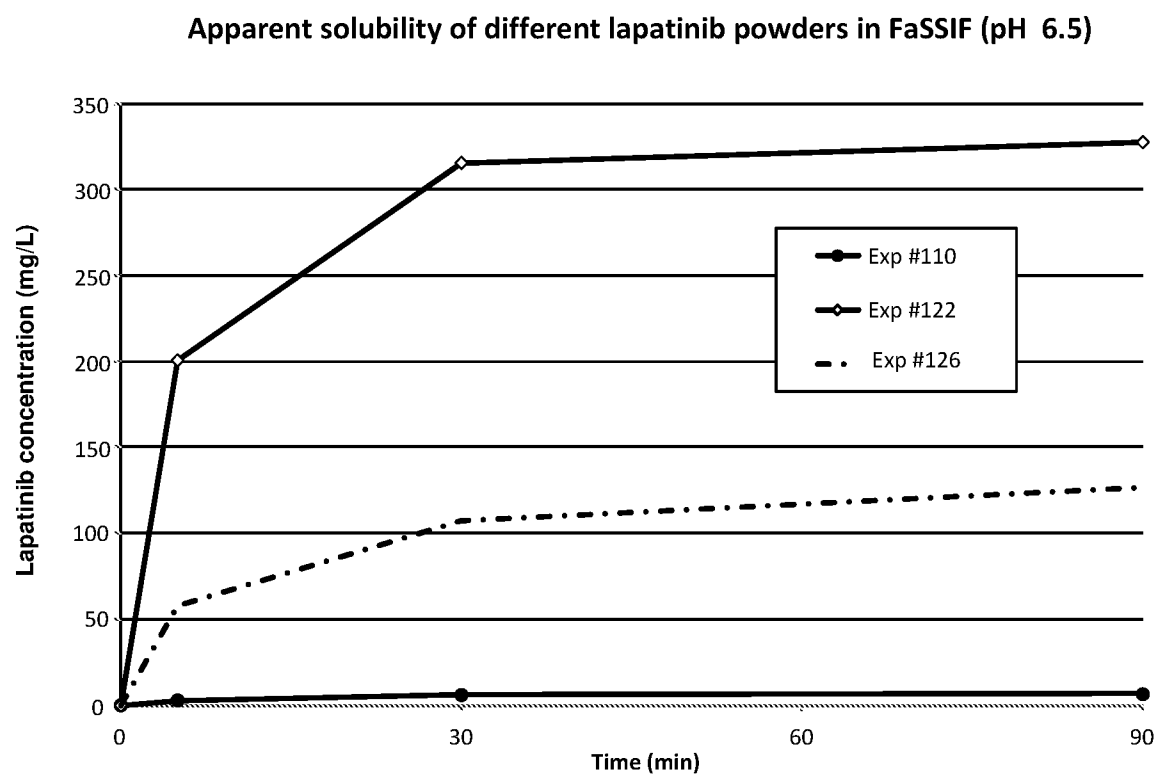


Figure 5

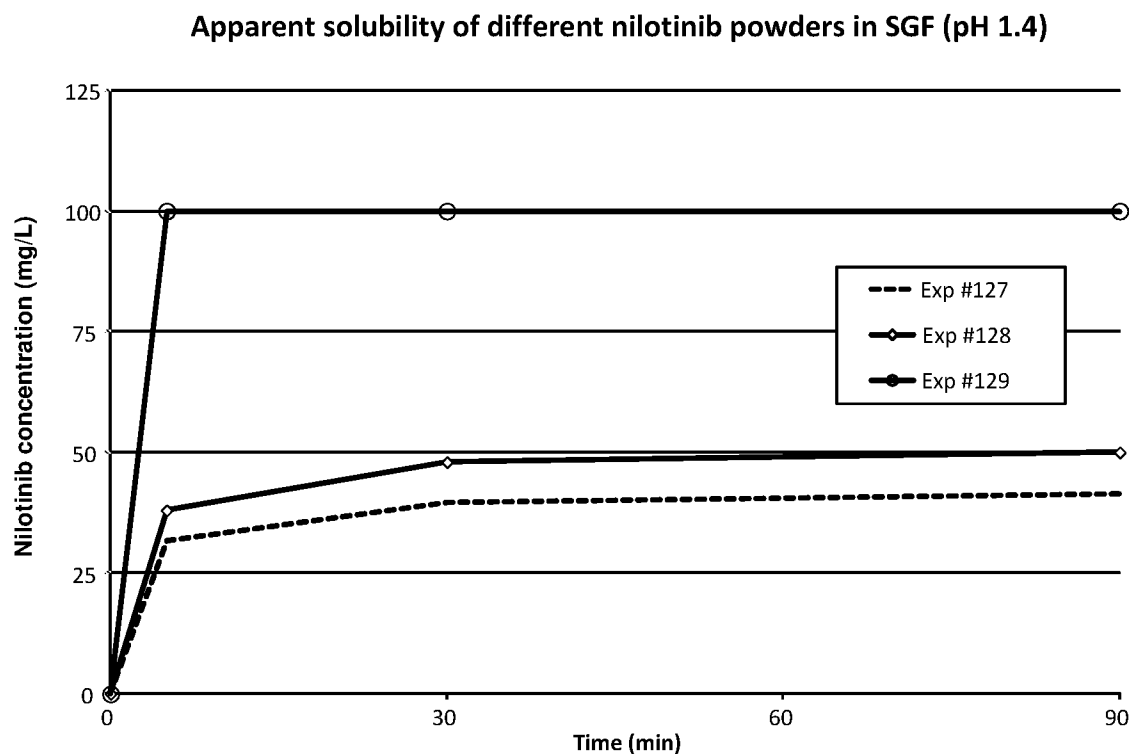


Figure 6

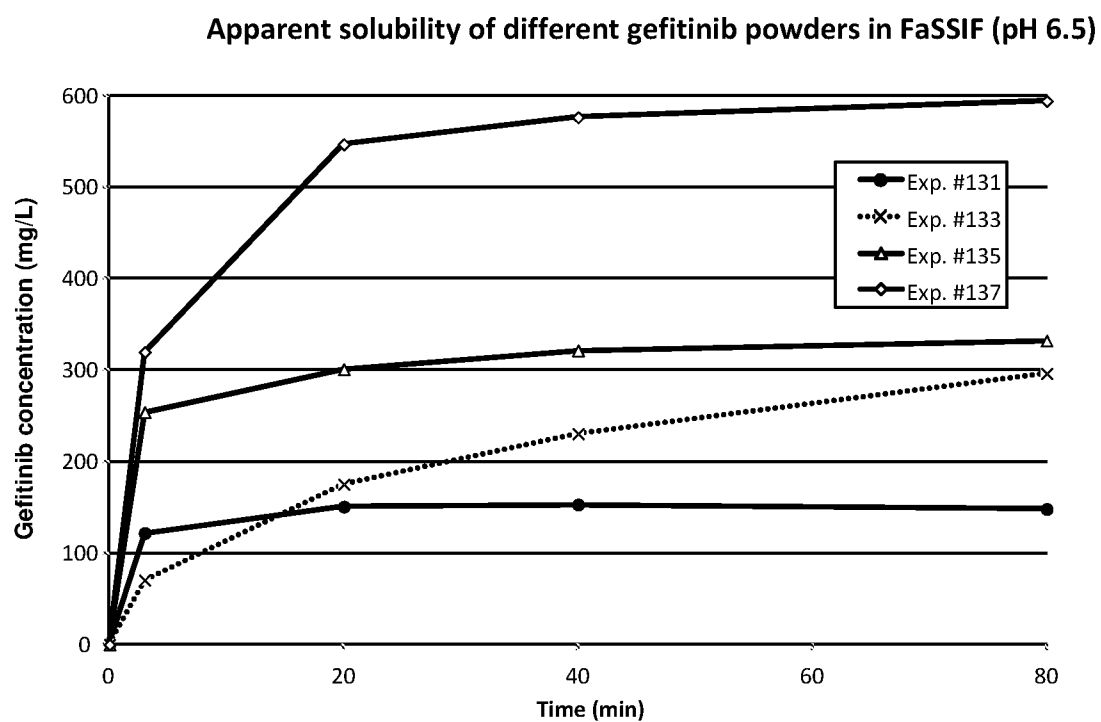


Figure 7

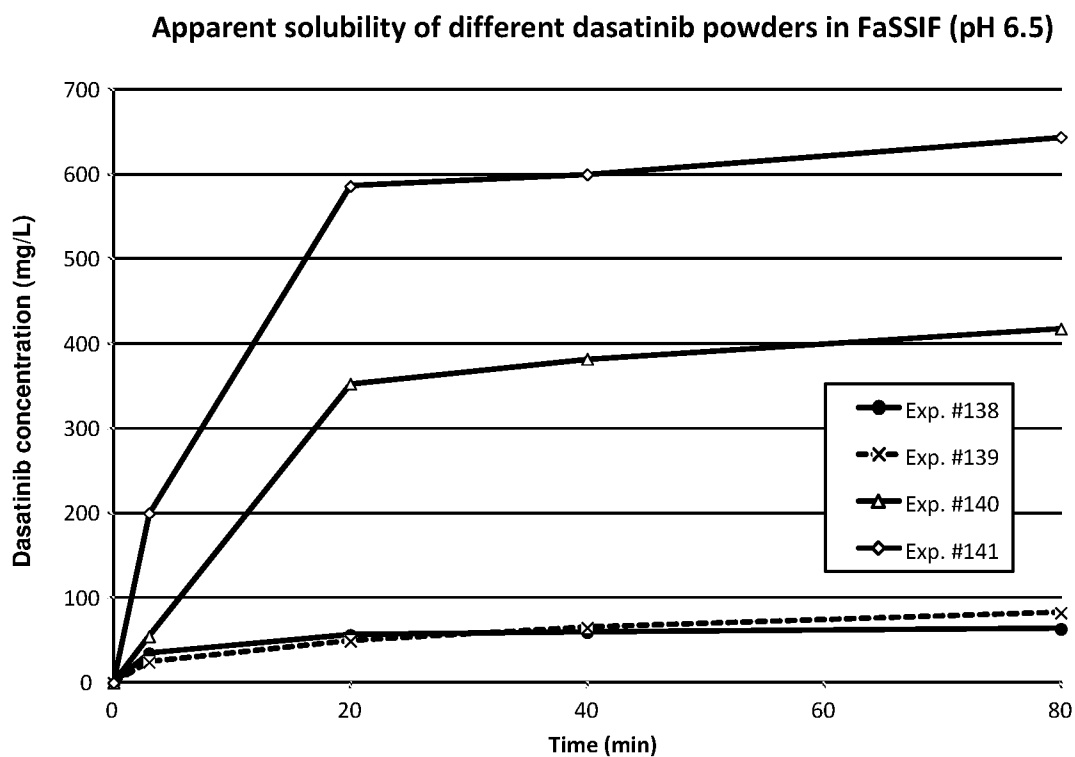


Figure 8

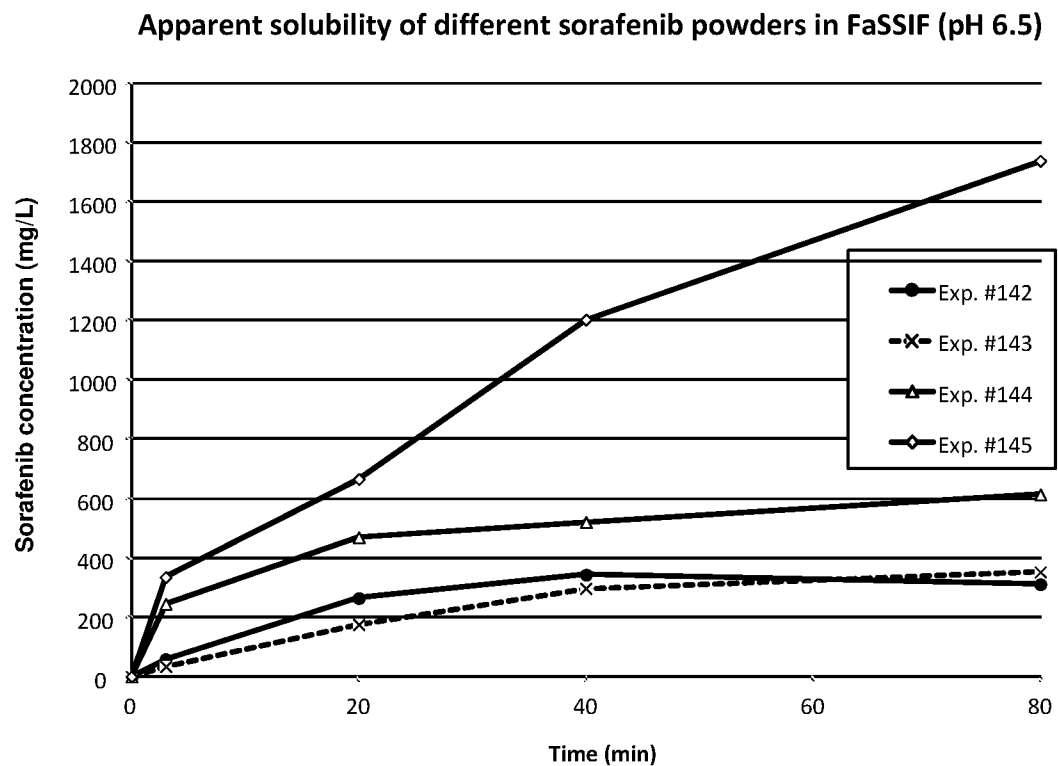


Figure 9

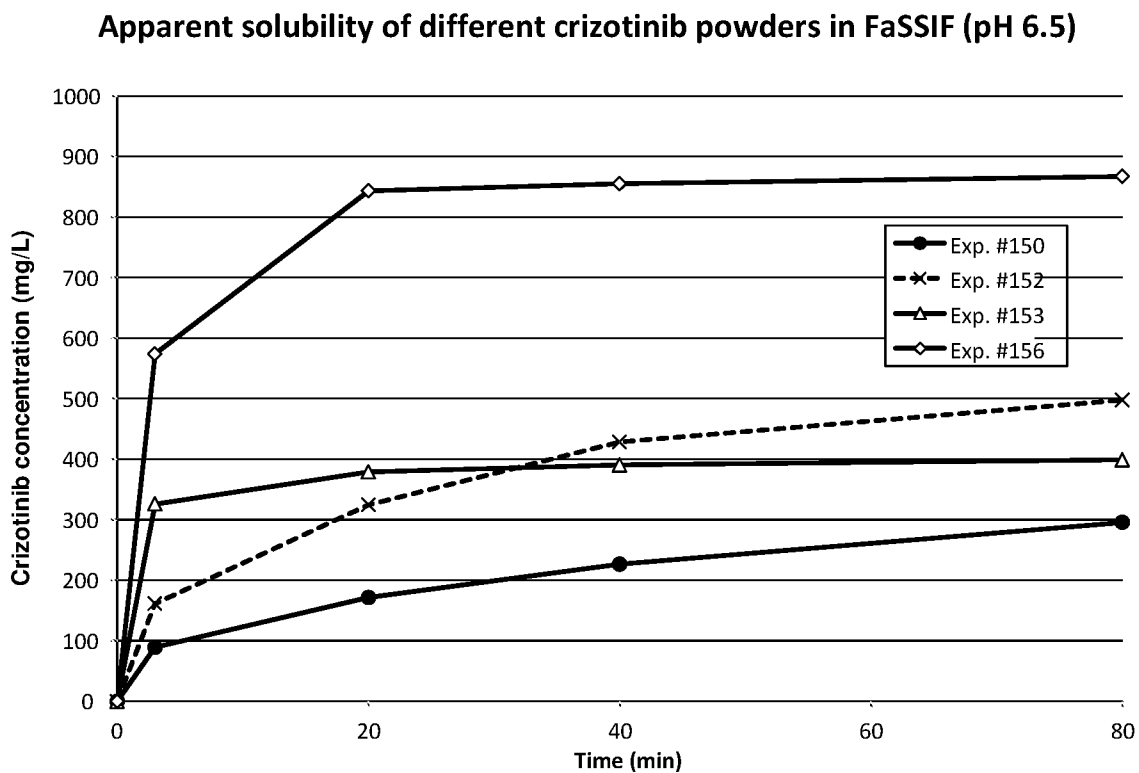


Figure 10

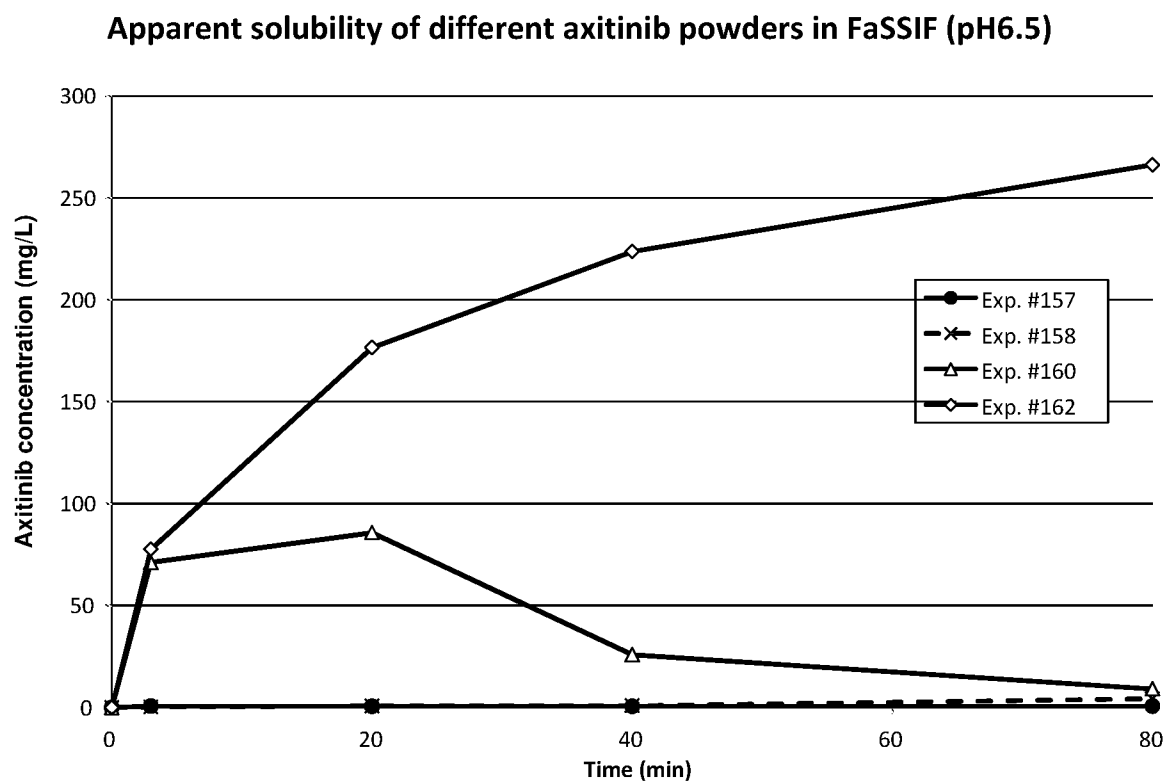


Figure 11

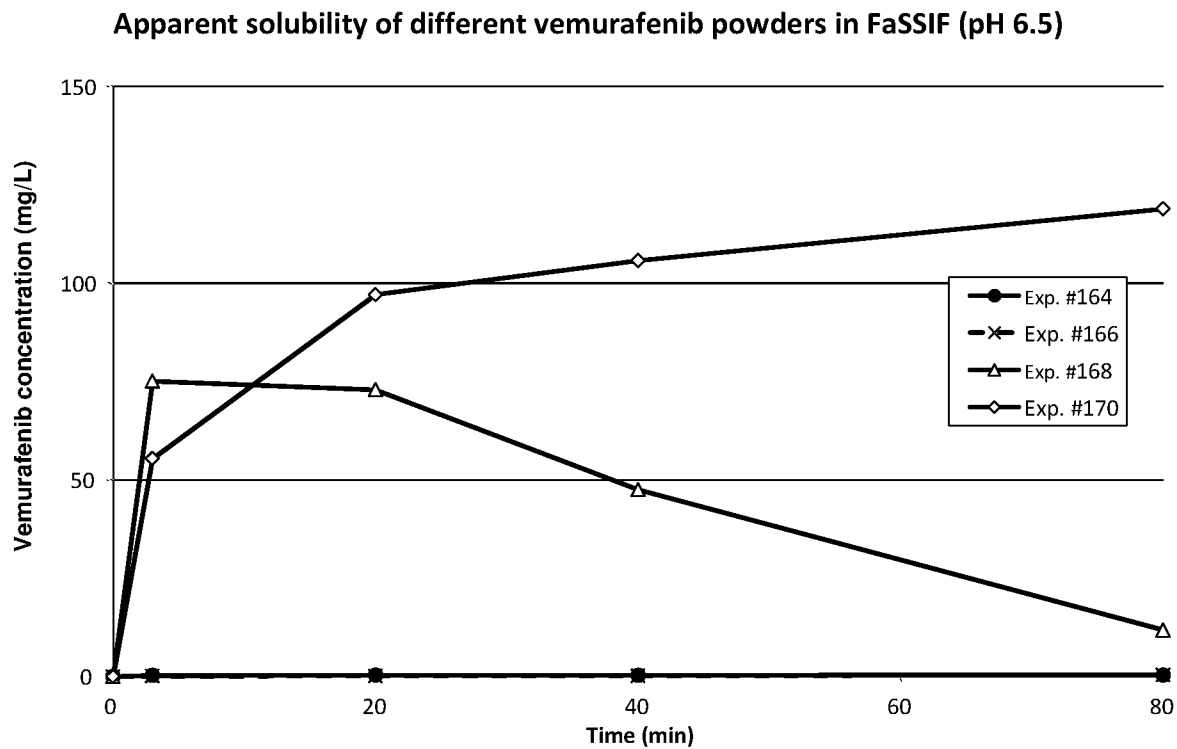


Figure 12

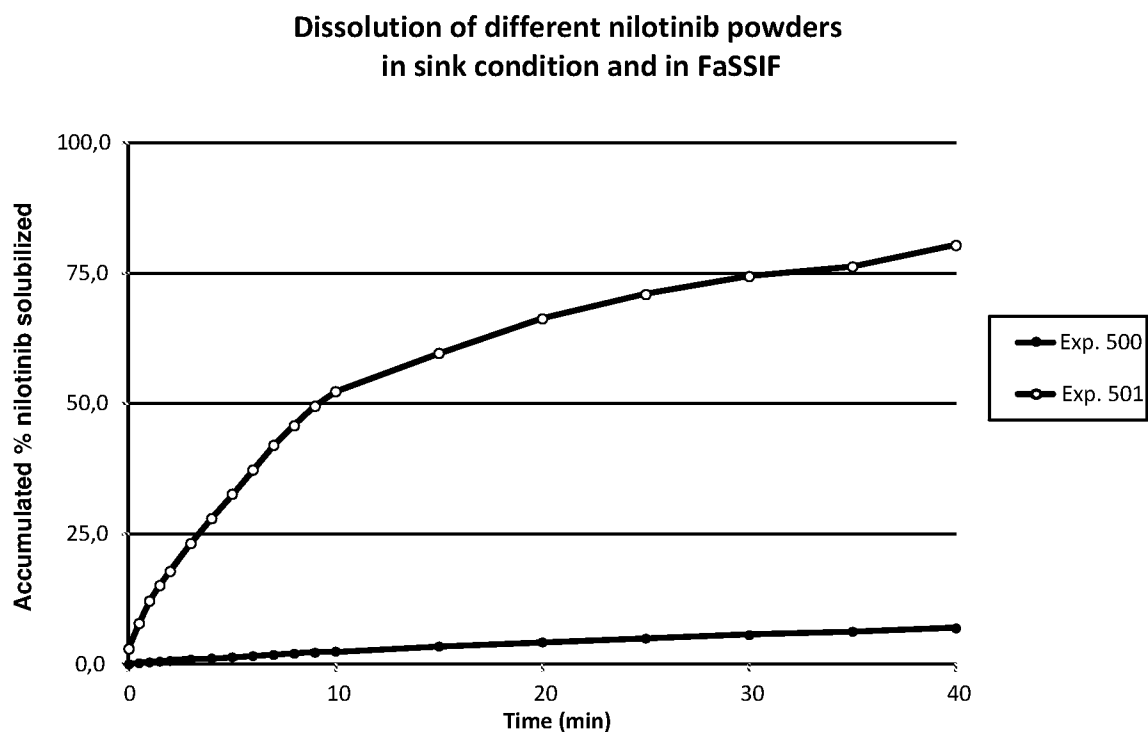


Figure 13

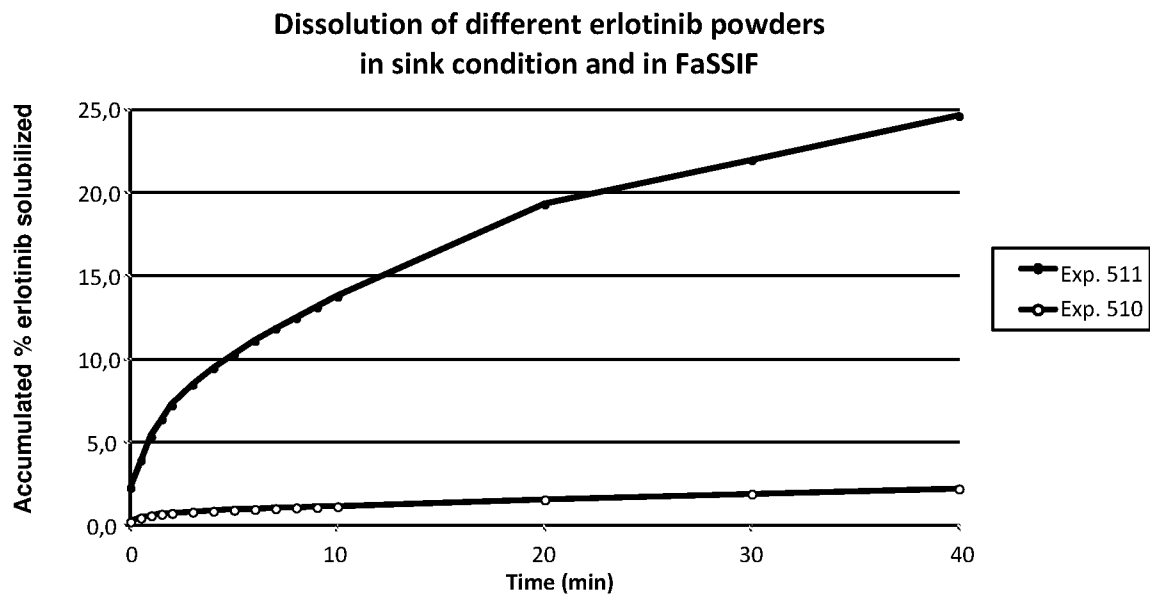


Figure 14

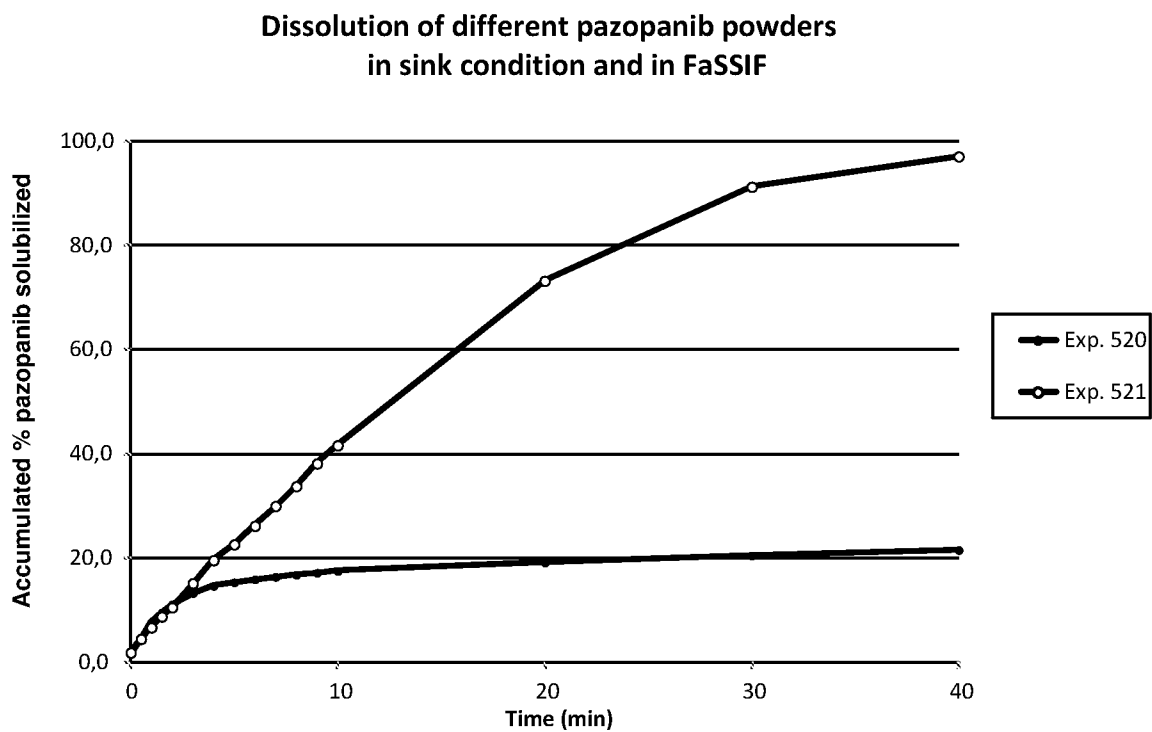


Figure 15

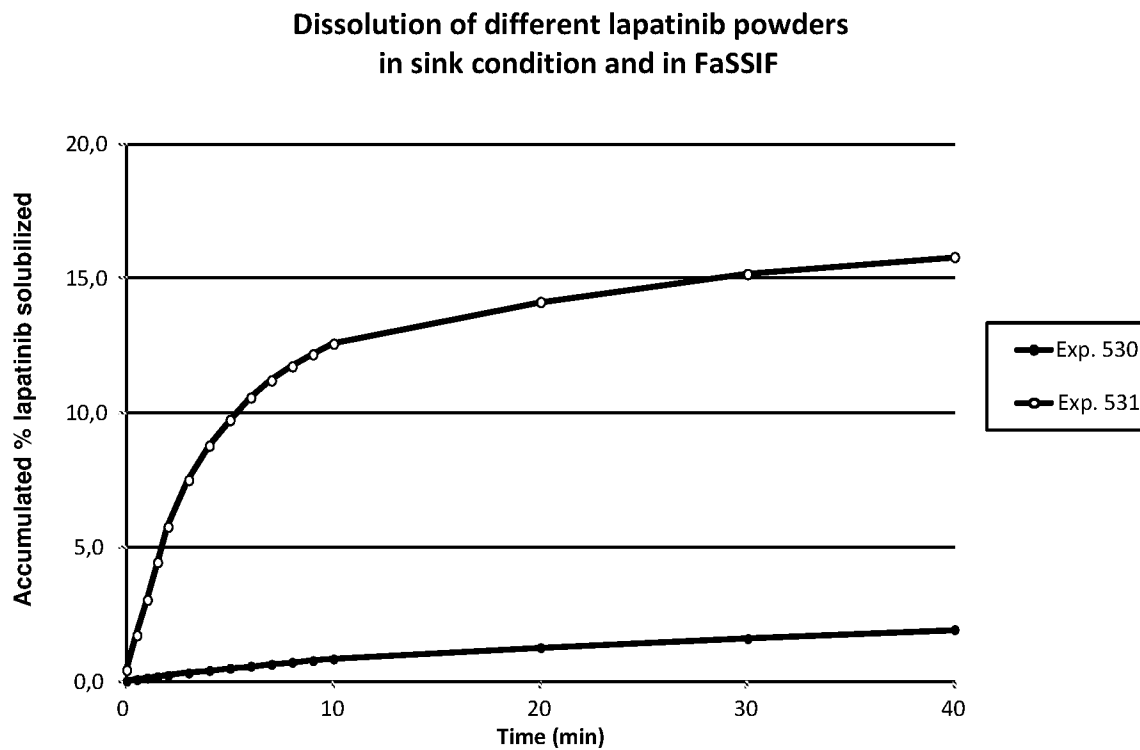


Figure 16

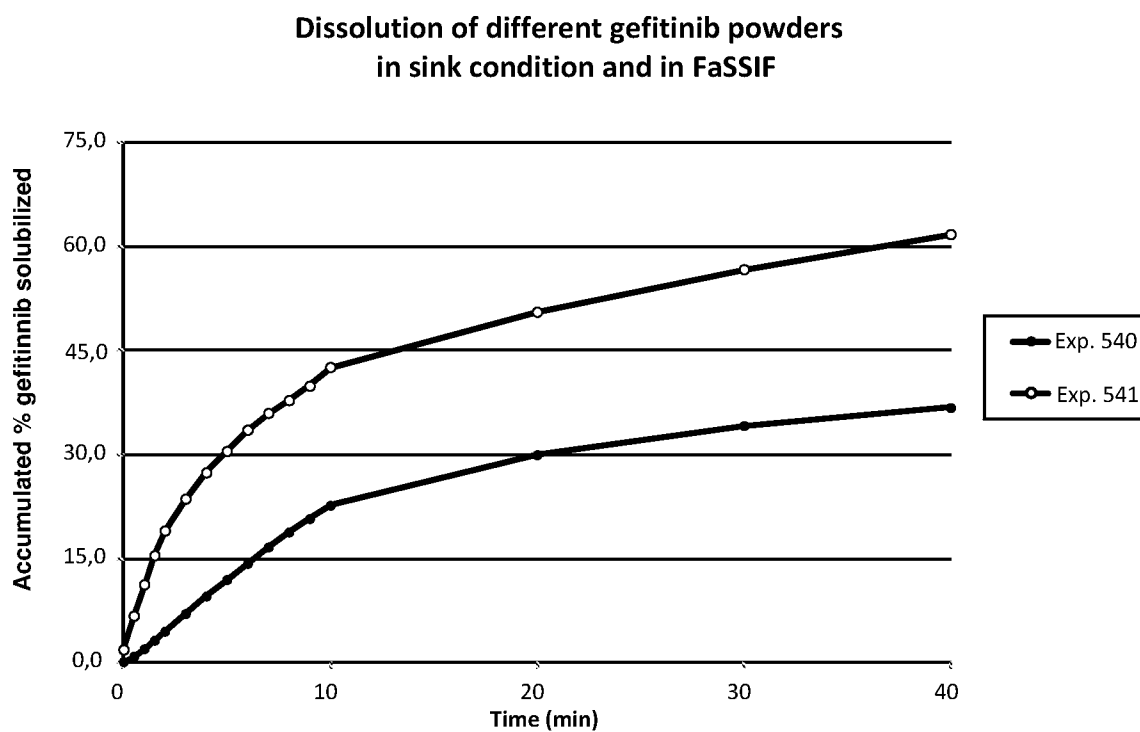


Figure 17

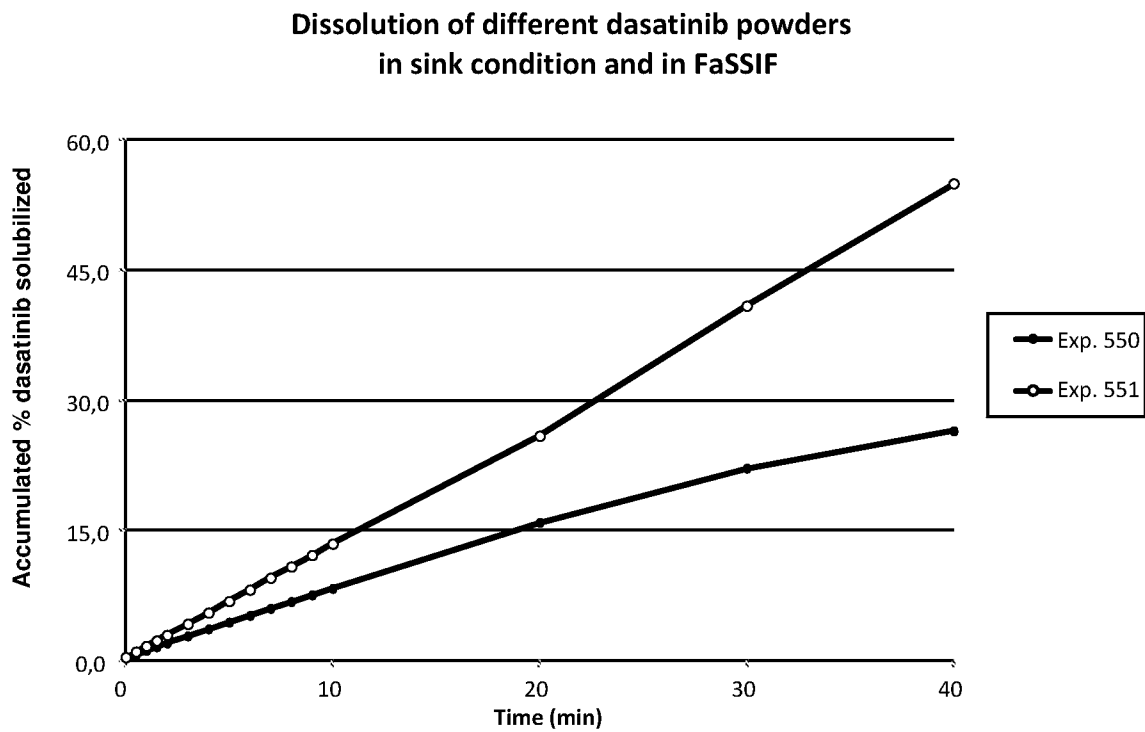


Figure 18

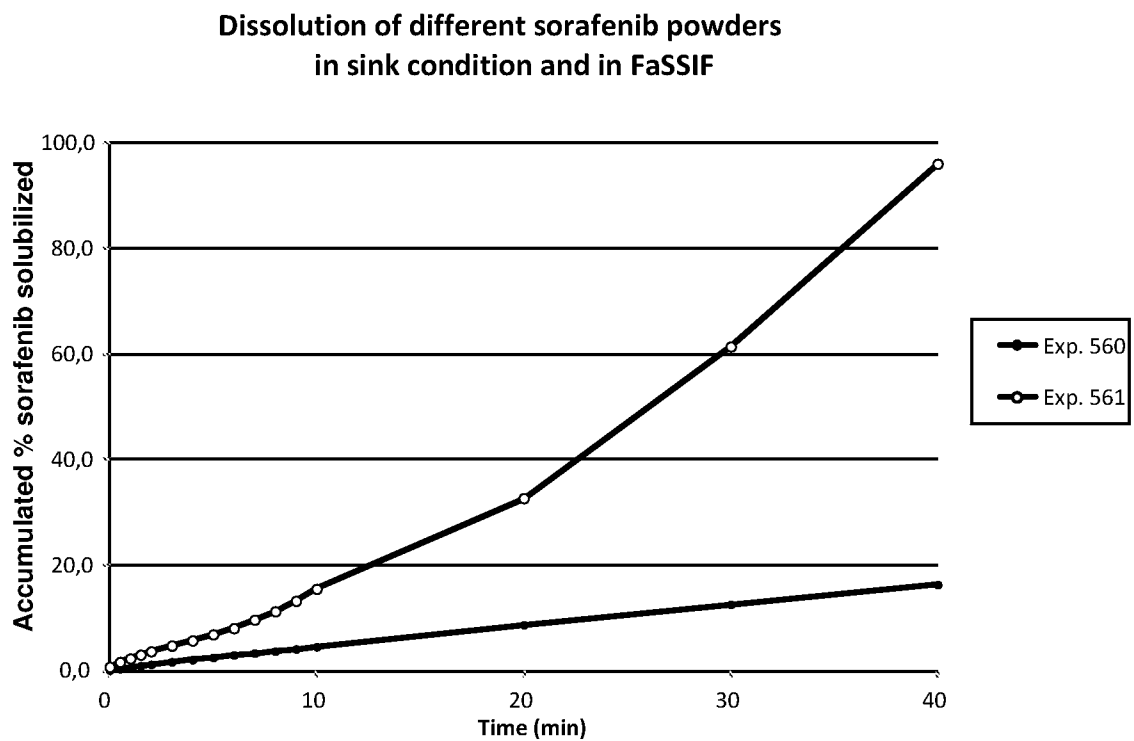


Figure 19

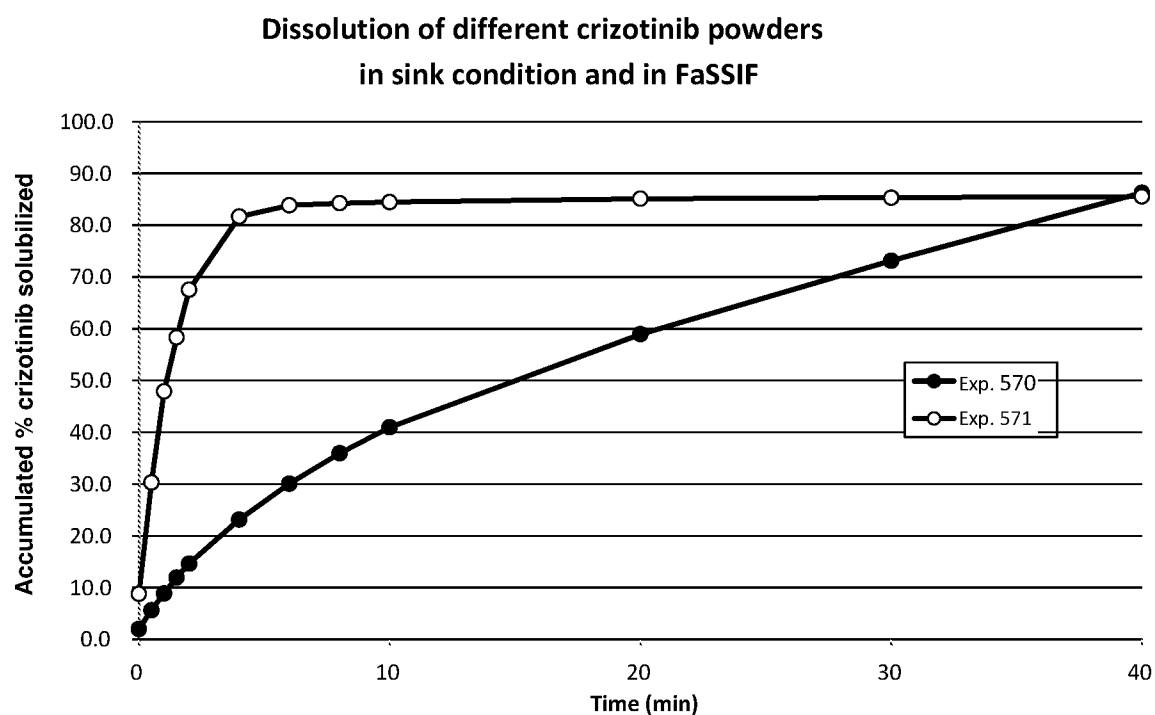


Figure 20

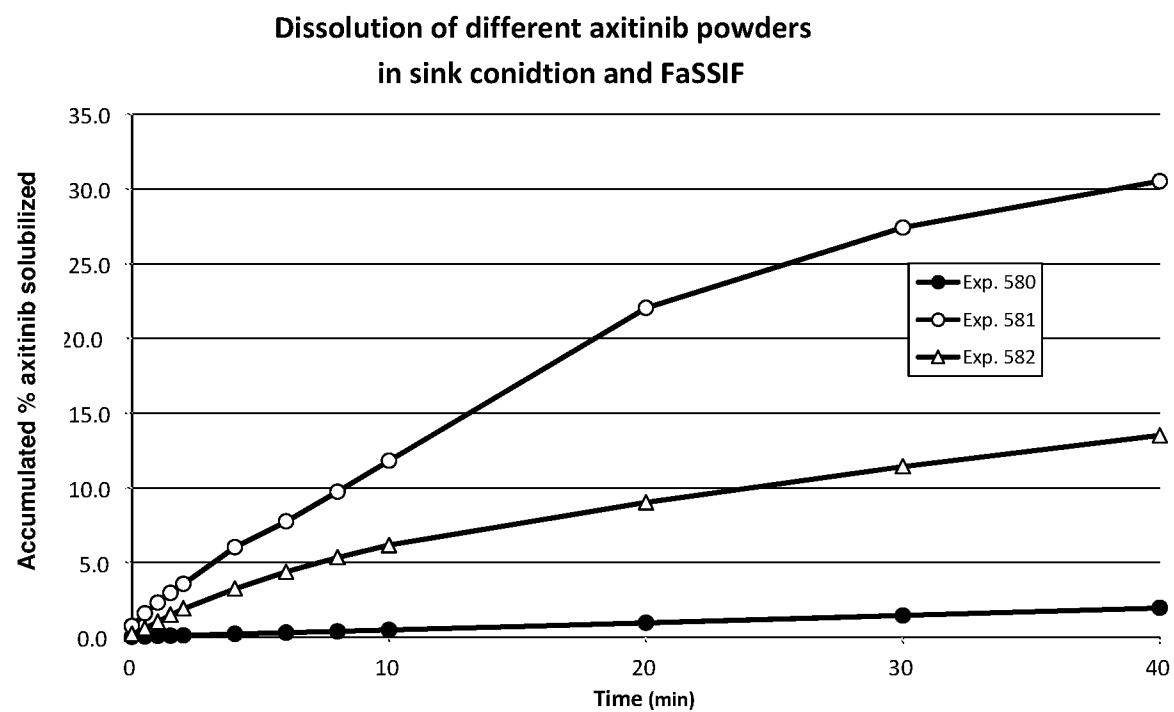


Figure 21

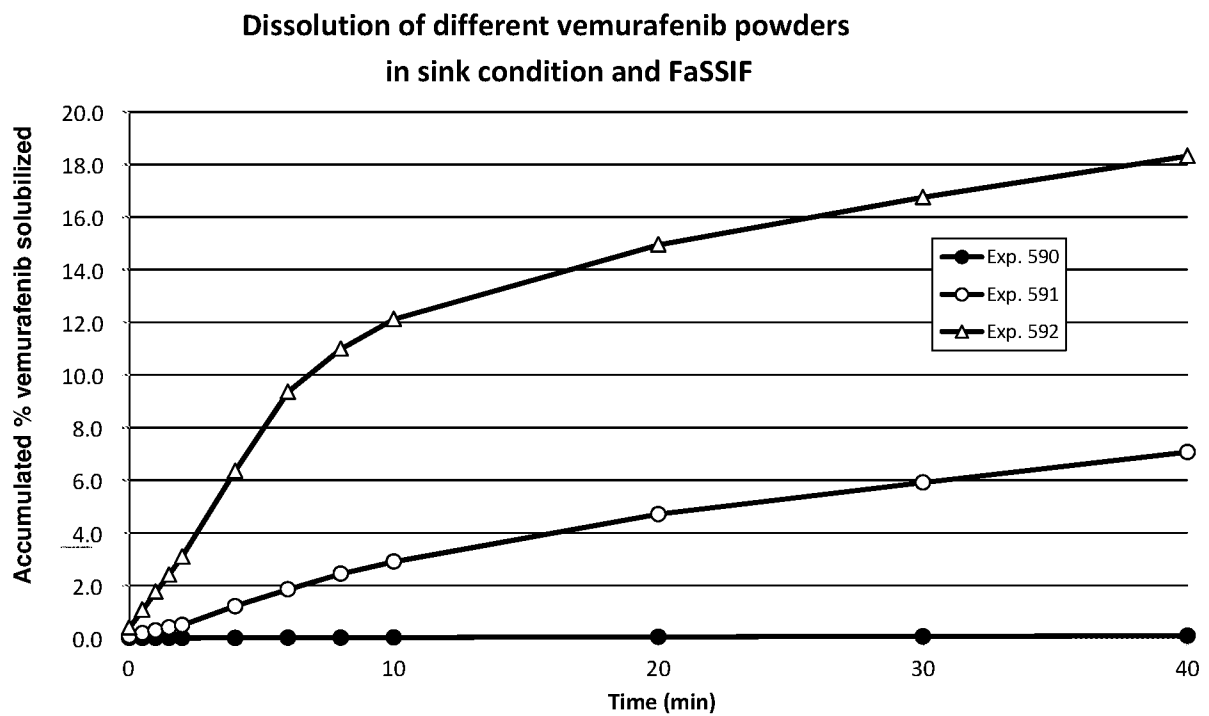


Figure 22

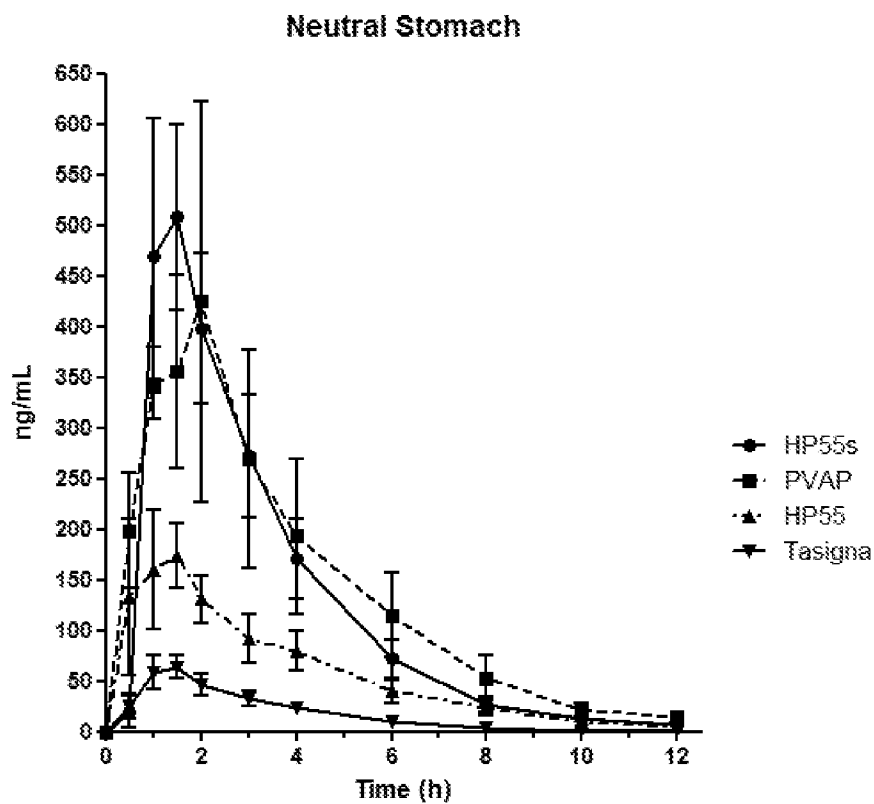


Figure 23

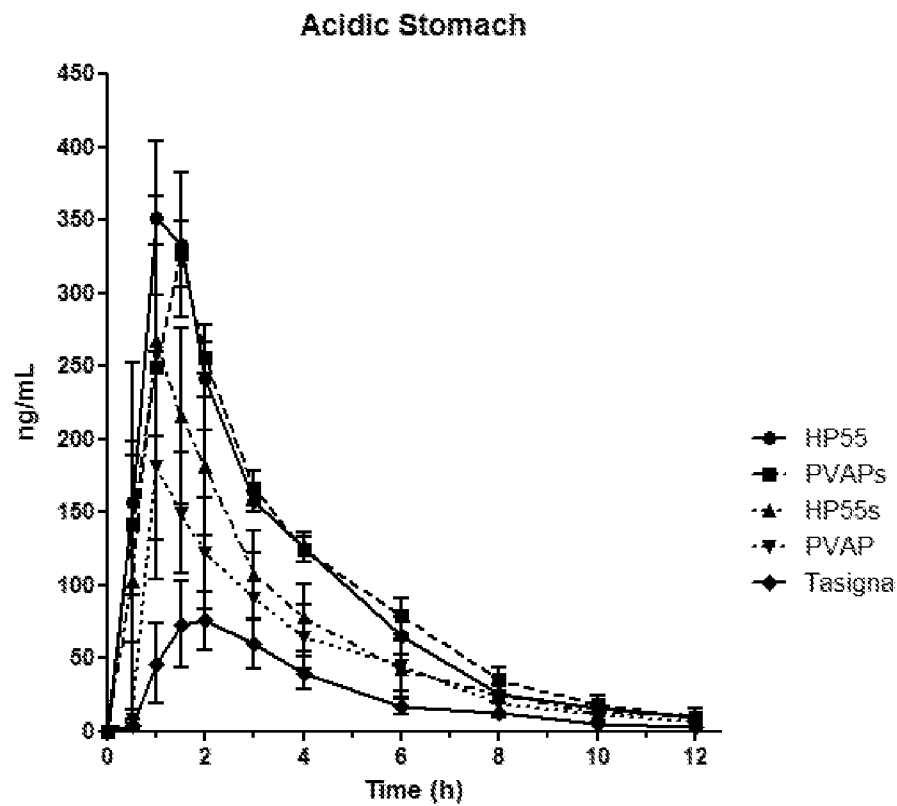


Figure 24

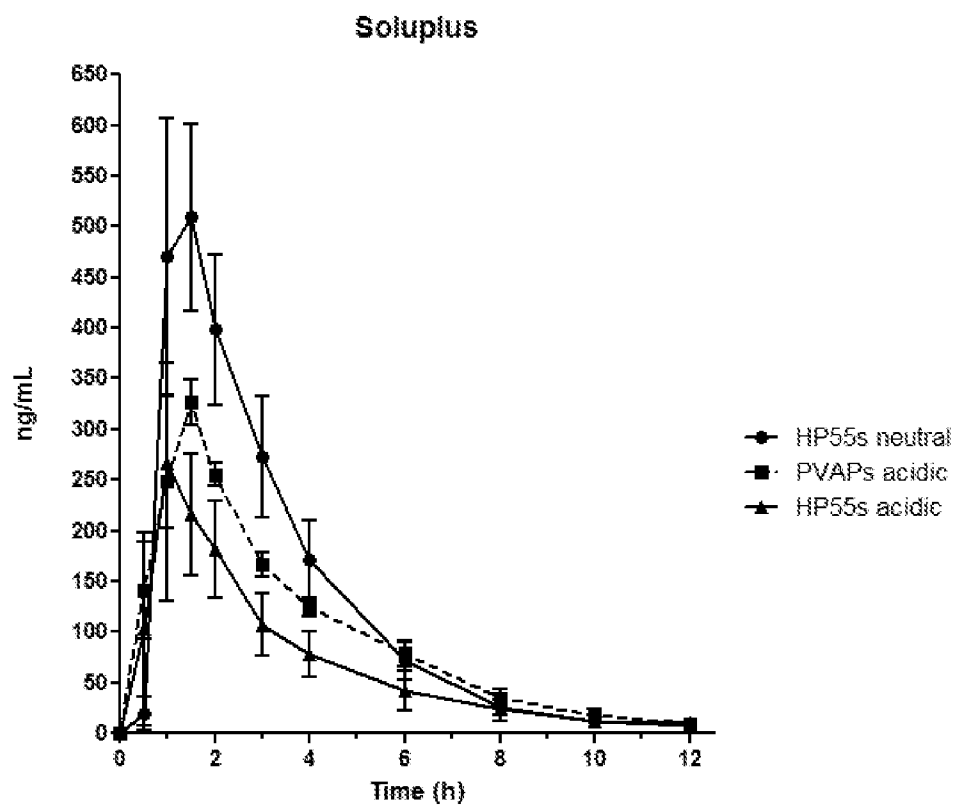


Figure 25

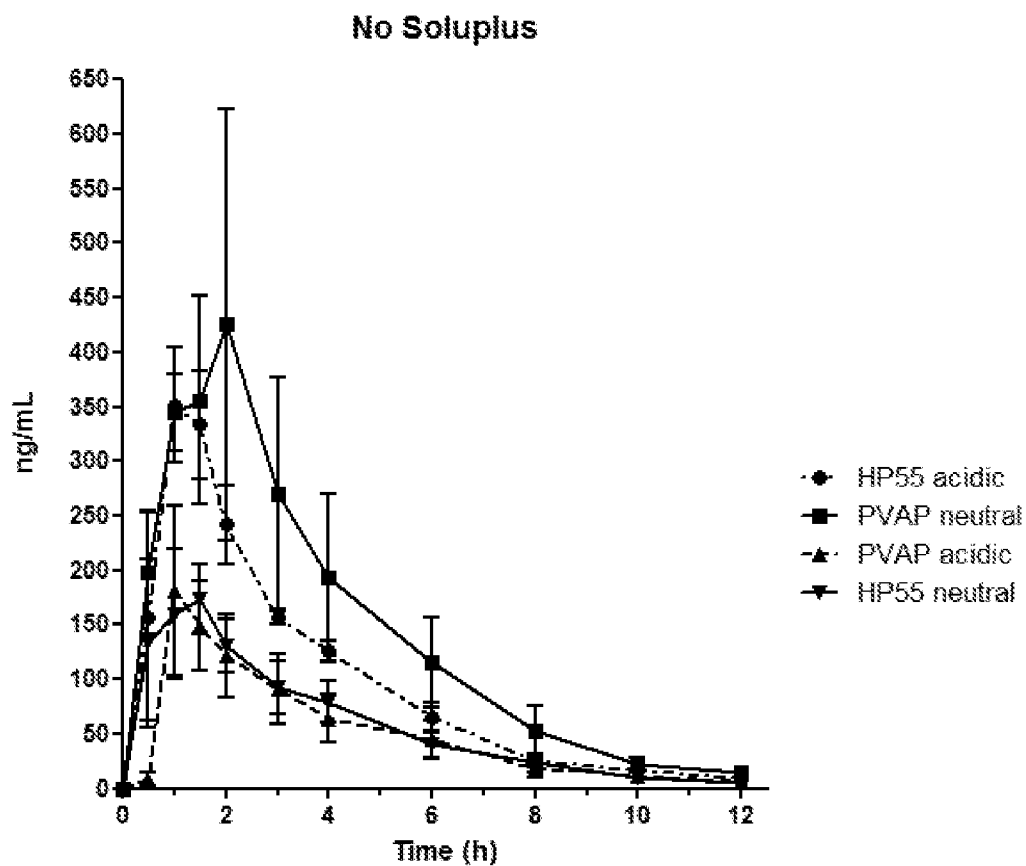


Figure 26

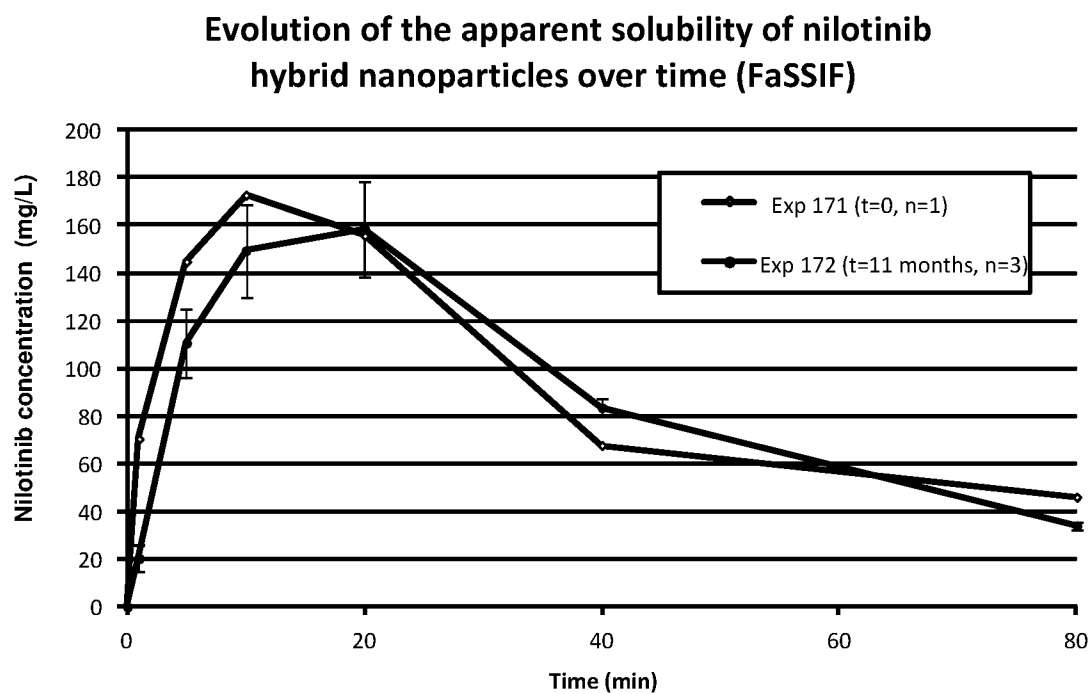


Figure 27