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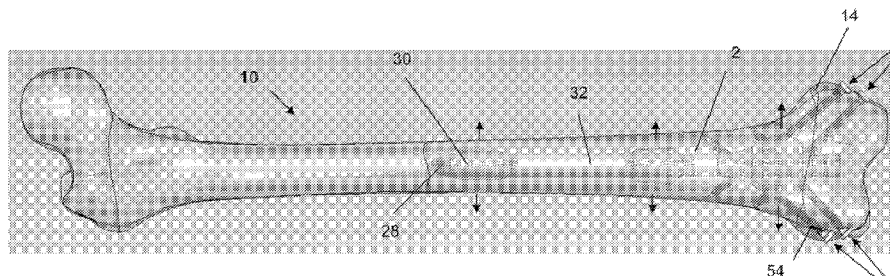


Fig. 19

(57) Abstract: A device for radial expansion in an endoluminal cavity in a bone is disclosed. The device can be used to treat bone fractures. The device can have a first radially expandable portion and a second radially expandable portion.

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1 TITLE OF THE INVENTION  
2 **EXPANDABLE ORTHOPEDIC DEVICE AND METHOD**

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8

9 CROSS-REFERENCE TO RELATED APPLICATIONS

10 **[0001]** This application claims priority to U.S. Provisional Application No. 61/022,613, filed 22  
11 January 2008, which is incorporated by reference herein in its entirety.

12  
13 BACKGROUND OF THE INVENTION

14 1. Field of the Invention

15 **[0002]** The present invention relates generally to a device and method for stabilizing bones and  
16 anchoring to bones and bone fragments.

17  
18 2. Description of Related Art

19 **[0003]** Figure 1 illustrates a longitudinally split femur bone **8** with the proximal (coronal) end on  
20 the right. The femur **10** is a long bone. Bones, such as femurs, have hard, dense cortical outer bone  
21 **34**, and softer, less dense cancellous inner bone **4** that forms a lumen within the shell of cortical  
22 bone **34**. Figure 2 illustrates the endoluminal cavity **6** formed by the cancellous bone **4**.

23 **[0004]** Broken bones, such as long bone breaks, may be treated with fixation. Rigid stabilization  
24 rods are often attached to the pedicles of the vertebrae (not shown) with fixation screws. The  
25 fixation screws can be driven into the cortical outer shell of the bone.

26  
27 SUMMARY OF THE INVENTION

28 **[0005]** An expandable orthopedic device is disclosed. The device can be a radially expandable  
29 attachment device. The device can be used for to therapeutically treat trauma injuries in bones, for  
30 example long bone fractures. The device can be fixed in the endoluminal cavity on two sides of a  
31 long bone break.

32 **[0006]** The device can have a structure that can radially expand inside a bone, for example in the  
33 endoluminal cavity of a long bone. For example, the device can have a stent-like expandable  
34 frame. The device can be implanted in the endoluminal cavity in a radially unexpanded  
35 configuration. The device can be radially expanded in the endoluminal cavity using a simple tool,  
36 both pump handles, rotational type tools (e.g., cams), or combinations thereof.

1 [0007] The devices can be made from metals, plastics, or combinations thereof, as disclosed infra.  
2 The device can be entirely metal, mixes of metal and plastic, entirely plastic, and the device can  
3 also have other polymers, agents, fillers and other materials disclosed infra. For example, the  
4 radially expandable portion of the device can be a first material (e.g., a first metal) and the  
5 remainder of the device can be primarily or entirely made from a second material (e.g., a second  
6 metal).

7 [0008] The expansion element can be configured to expand through cancellous bone, and stop  
8 when the expansion element contacts hard cortical bone and/or sufficient mechanical resistance.  
9 The expansion element can be configured to expand partially or completely into cortical bone, for  
10 example to anchor the expansion element into the cortical bone.

11 [0009] The device can be configured to apply a high level of radial force to the inner endoluminal  
12 wall of a bone or a low level of radial force.

13 [0010] The device can be designed to stop radially expanding based on displacement (e.g., an  
14 internal stop or extent of the length of the radial expansion). The device can be configured to fail  
15 mechanically once the device receives a specific mechanical load or resistance, for example for  
16 removal or replacement, and/or to prevent the device from over-stressing the bone (e.g., for the  
17 device to fail before the bone fails).

18 [0011] The device can contour to the inside of the cortical surface (i.e., outside of the endoluminal  
19 cavity) during radial expansion and can anchor to the cortical surface.

20 [0012] Part or all of the outside surface of the device can be textured (e.g., teeth, barbs, hooks,  
21 spikes, holes, ridges, knurls, combinations thereof), for example to increase anchoring or improve  
22 in-growth of the bone into or towards the device.

23 [0013] The textured surface can be configured to match the required loading. For example, the  
24 ridges can be oriented along the longitudinal axis of the device, for example, to resist torque loads  
25 on the device by pressing the ridges against the cortical bone accordingly (e.g., in the direction of  
26 the torque, producing additional resistance to the torque). The ridges can be oriented perpendicular  
27 to the longitudinal axis, for example to resist tensile or compressive loads on the device by pressing  
28 against the cortical bone accordingly.

29 [0014] The device can stabilize bone fragments, for example by acting as an endo-scaffold (i.e., a  
30 scaffold from within the bone) when in an expanded and/or contracted configuration.

31 [0015] One or more fixation screws can be screwed through bone and into the device – for  
32 example when the device is used as an endo-scaffold. The screws can, for example, brace or align  
33 the device against or with the bone. By fixing the bone to the device, the bracing element (e.g.,  
34 fixation screw) can stabilize the bone by pushing the bone radially inward toward the central axis of  
35 the bone (e.g., not to one side or the other, for example like a typical external fixation plate or rod).  
36 The fracture or bone fragments can be pushed towards the device in the endoluminal cavity. The

1 screws used to screw bone fragments directly onto the device can be lag screws, for example with a  
2 distal machine thread.

3 **[0016]** The device can have any or all elements from any of the devices and/or be used with any  
4 method disclosed in U.S. Provisional Application No.: 60/906,791, filed 12 March 2007, and PCT  
5 App. No. US2008/003421 which are incorporated by reference herein in their entireties. The  
6 expandable sections can be made from any configuration (e.g., springs), not just radially expanding  
7 bending struts.

8 **[0017]** The device can be partially or completely hollow. For example, the device can be hollow  
9 along the length of the expandable section. The hollow section of the device can be filled with one  
10 or more cement, fillers, glues, and/or an agent delivery matrix and/or a therapeutic and/or  
11 diagnostic agent. Any of these cements and/or fillers and/or glues can be osteogenic and  
12 osteoinductive growth factors.

13 **[0018]** The device can be implanted anti-grade, retrograde, or constructed from segments from the  
14 center of a bone.

15 **[0019]** The device can be completely or partially bare or covered. The device can have a liner  
16 made from a thin film or fabric (e.g., plastic, metal). For example, the liner can control filler flow  
17 and/or improve screw anchoring (e.g., by attaching the fixation screw).

18 **[0020]** The device can be recovered and removed, or repositioned or otherwise adjusted within the  
19 endoluminal cavity.

20 **[0021]** The device can anchor against the cortical bone, for example reducing device motion. The  
21 device can be configured to be rigid or flexible.

22 **[0022]** The device can have one or more radially expandable sections. The expandable sections  
23 can be on one or both ends of the implants. The expandable sections can be located along the  
24 length of the device at regular or varying length intervals.

25 **[0023]** The expandable sections can be expanded in any direction (e.g., distal first, proximal last)  
26 or out of order along the length of the device. Some expandable sections can be left unexpanded.  
27 The expandable sections can be expanded in a sequence to best stabilize the fracture during  
28 deployment of the device.

29 **[0024]** The expandable sections can be used to move the fractured segments of the bone. For  
30 example, the expandable section can then be unexpanded and the device moved after the fractured  
31 segment of the bone is moved as desired.

32 **[0025]** The device, for example via the expandable sections, can be used to remove cancellous  
33 bone, for example by reaming the endoluminal bone cavity with the expandable section in a radially  
34 expanded and/or radially contracted configuration.

1 [0026] A main stem of a joint replacement or resurfacing device can be anchored by having one or  
2 more expandable sections in the main stem. The expandable section can be filled with a filler or  
3 other material disclosed herein.

4 [0027] The device can be sized and shaped to fit big and small bones (e.g., finger, femurs).

5 [0028] The device can have one or more external guides, for example ridges, rails, threaded holes,  
6 or combinations thereof, to guide the screws into the device.

7 [0029] The expandable sections can be expanded by inflating a balloon and/or screw jack (e.g., to  
8 bring the longitudinal ends of the expandable section nearer to each other), and/or expanding a  
9 wedge-jack inside of the expandable sections.

10 [0030] The fixation screws can have a polyaxial washer head, for example, to distribute stresses.  
11 The fixation screws can be linked to one another by a thread, suture, rod, plate, strap or  
12 combinations thereof.

13 [0031] The screws can pass through one or more (e.g., two) of the walls of the device. For  
14 example, the screw can enter one side and exit the opposite side of the device. A single screw can  
15 anchor through cortical bone on substantially opposite sides of the endoluminal cavity.

16 [0032] The fixation screws can have a distal thread. The distal thread can attach into a cell hole of  
17 the expandable sections.

18 [0033] The diameter of the screws can be sized to match the diameter of the cell hole.

19 [0034] The expandable section can have one or more layers of walls. The walls can have  
20 interconnected struts defining expandable cells. The struts can attach to each other at deformable,  
21 resilient and/or rigid joints. Any or all of the remainder of the device can have one or more walls.

22 [0035] The device can be configured so the (longitudinal axis of the) device can be straight and/or  
23 curved. The device can be configured to match the topography (i.e., shape) of the endoluminal  
24 cavity defined, for example, by the inner wall of the cortical bone. The device can be used to  
25 anchor a mesh, suture, or another implant. The device can be curved before radial expansion. The  
26 device can be curved and/or bent during radial expansion.

27 [0036] The expandable sections can expand to a round, square, triangular, contoured to the inner  
28 wall surface, or combinations thereof cross-sectional configuration. The expandable section can  
29 expand into a sphere, rectangle, cube, or contoured any shape to improve anchoring inside a bone.

30 [0037] The device can be used to fill a bone void (e.g., for vertebroplasty (also known as  
31 kyphoplasty), tumor therapy, trauma therapy).

32 [0038] Layers of metals, plastic,...

33 [0039] The device can be any length, for example sized to fit a scaphoid or femur.

34 [0040] The device can have expandable sections that can be configured to expand radially,  
35 planarly, curvedly, with corresponding wedges, as a polygon, or combinations thereof.

36 [0041] The expandable sections can self-expand (e.g., resilient expansion).

1 [0042] The device can be used with screws, wire, sutures, or combinations thereof. The  
2 expandable section can have many holes or few holes.

#### 4 SUMMARY OF THE FIGURES

5 [0043] Figures 1 and 2 are longitudinal sectional views of a femur.

6 [0044] Figure 3 illustrates a perspective view of a longitudinally sectioned femur.

7 [0045] Figure 4 is a sectional view of a femur with the cancellous bone removed.

8 [0046] Figures 5 and 6 illustrate a femur.

9 [0047] Figure 7 illustrates a variation of the device in a contracted configuration at a target site  
10 with the bone shown in partial see-through.

11 [0048] Figure 8 illustrates a variation of the device in an expanded configuration at a target site  
12 with the bone shown in partial see-through.

13 [0049] Figures 9a through 9c are radiographical images a variation of a method for deploying the  
14 device.

15 [0050] Figures 10a and 10b are radiographical images of side and end views, respectively, of a  
16 variation of the device at a target site in a long bone.

17 [0051] Figures 11a and 11b are radiographical images of a variation of the device at a target site in  
18 a radially expanded configuration.

19 [0052] Figures 12a and 12b are radiographical images of a variation of the device at a target site in  
20 a radially expanded configuration.

21 [0053] Figure 13 illustrates a femur.

22 [0054] Figure 14 illustrates a method of inserting a variation of the device into a femur.

23 [0055] Figure 15 is a variation of close-up A-A of Figure 14.

24 [0056] Figure 16 illustrates a variation of close-up A-A before the bone is closed (i.e., the fracture  
25 is reduced) and stabilized.

26 [0057] Figure 17 illustrates Figure 16 with the bone substantially closed and stabilized.

27 [0058] Figure 18 illustrates a femur.

28 [0059] Figures 19 and 20 illustrate a variation of the device at a target site with the bone shown in  
29 partial see-through.

30 [0060] Figure 21 illustrates that the variation of the device at a target site.

31 [0061] Figures 22a, 22b and 22c are progressively more magnified close-ups of the distal head of  
32 the femur in partial-see though with a device implanted in the femur.

33 [0062] Figure 23 illustrates an outside view of a variation of the device being inserted and  
34 expanded.

35 [0063] Figure 24 is a radiographical image of a variation of the device in an expanded  
36 configuration at a target site.

1 [0064] Figures 25a and 25b illustrate progressively more magnified close-ups of the device in a  
2 carpal bone with the bone shown in partial see-through.

3 [0065] Figures 26a and 26b illustrate progressively more magnified close-ups of the device in a  
4 wrist bone with the bone shown in partial see-through.

5 [0066] Figures 27a and 27b illustrate variations of transverse cross-sections of the device in  
6 unexpanded and expanded configurations, respectively.

7 [0067] Figures 28a through 28d are radiographical images of a variation of a method for removing  
8 the device from a target site.

9 [0068] Figures 29a through 29d are side views of a variation of a method for removing the device  
10 and surrounding tissue.

11 [0069] Figures 30a through 30d illustrate variations of transverse cross-section C-C of Figure 10a.

12 [0070] Figures 31a and 31b are longitudinal sectional views of variations of the device in an  
13 expanded configuration with a locking rod.

#### 14 15 DETAILED DESCRIPTION OF THE INVENTION

16 [0071] Figure 3 illustrates that all or part of the cancellous bone 4 can be removed from the  
17 endoluminal cavity 6 of a bone 8, such as a long bone 8 such as the femur 10. The cancellous bone  
18 4 can be removed with a finger (as shown), if the cancellous bone 4 is sufficiently soft, or with a  
19 reamer or other tool. Figure 4 illustrates a femur 10 with the cancellous bone 4 removed from the  
20 endoluminal cavity 6.

21 [0072] Figure 5 illustrates three exemplary indications for use of the device include trochanteric  
22 fractures 1, mid-shaft fractures 2, distal fractures 3, and combinations thereof. Figure 6 illustrates  
23 the greater trochanter 16 and femoral head 12. The trochanter fracture 14 can bisect the greater  
24 trochanter 16.

25 [0073] Figure 7 illustrates that multiple expandable attachment devices 2 can be used in a  
26 procedure. For example, a first expandable attachment device 22 can be inserted through the collar  
27 20 of a second expandable attachment device 24 to attach the two devices together.

28 [0074] The first expandable attachment device 22 can be inserted into the femoral head 12. The  
29 second expandable attachment device 24 can be inserted along the endoluminal cavity 6 of the  
30 femoral shaft.

31 [0075] The first expandable attachment device 22 can have a traumatic screw or otherwise  
32 sharpened tip 26. The screw tip 28 can be turned into the bone 8 to help drive and seat the  
33 expandable attachment device 2 against the bone 8.

34 [0076] Either or both (shown as just the second) expandable attachment devices 22, 24 can have  
35 one or more radial expandable sections 30 and radial unexpandable sections 32. Figure 8 illustrates  
36 that all (as shown) or some of the radial expandable sections 30 can be radially expanded after (or

1 before – not shown) the expandable attachment device 2 is inserted into the bone 8. The expanded  
2 expandable sections 30 can secure one or both expandable attachment devices 22, 24 to the inside  
3 of the cortical bone 34. At least one of the expandable sections 30 (e.g., the expandable section 30  
4 of the first attachment device 22) can be on a first side of the fracture 14, and at least one of the  
5 expandable sections 30 (e.g., both expandable sections 36, 38 of the second attachment device 24)  
6 can be on a second side of the fracture 14.

7 [0077] Figure 9a illustrates that access to the endoluminal cavity 6 can be created by reaming  
8 through the cortical bone 34 and remaining out some or all of the cancellous bone 4.

9 [0078] Figure 9b illustrates that the second expandable attachment device 24 and the first  
10 expandable attachment device 22 can be inserted into the bone 8. The first expandable attachment  
11 device 22 can be inserted into the bone 8 after the second expandable attachment device 24, for  
12 example to insert the first expandable attachment device 22 through the collar 20 (or other  
13 attachment element) of the second expandable attachment device 24. Insertion of both expandable  
14 attachment devices 22 and 24 is shown by arrows.

15 [0079] Figure 9c illustrates that the first expandable attachment device 22 can be further inserted  
16 through the bone 8, for example by rotating and pushing the first expandable attachment device 22  
17 to utilize the screw tip 28 to drill through the bone 8. The expandable section 30 on the first  
18 expandable attachment device 22 (and any other expandable sections 30 desired) can then be  
19 radially expanded, as shown by arrows.

20 [0080] Figure 10a illustrates a lateral view of the femur 10 with an expandable attachment device  
21 2 inserted into the endoluminal cavity 6 and the expandable section 30 in a radially expanded  
22 configuration. The expandable section 30 can conform to the shape of the endoluminal cavity 6  
23 and can secure the expandable section 30 to the cortical bone 34. The expandable section 30 can  
24 have struts 40 that can define cells 42 (e.g., openings). The struts 40 can be joined to each other at  
25 joints. The struts 40 can be resiliently and/or deformably flexible and/or the joints can be  
26 resiliently and/or deformably flexible.

27 [0081] Figure 10b illustrates an axial view of the femur 10 with the expandable attachment device  
28 2 inserted. Figure 10b illustrates a variation of transverse cross-section C-C of Figure 10a.

29 [0082] Figures 11a and 11b illustrate the expandable attachment device 2 deployed in an  
30 osteopenic hip (i.e., in the femur 10). Figures 12a and 12b illustrate the expandable attachment  
31 device 2 deployed in a healthy hip (i.e., in the femur 10).

32 [0083] Figure 13 illustrates that a fracture 14 can be in the femur shaft 44. Figures 14 and 15  
33 illustrate that the expandable attachment device 2 can be removably attached to a deployment tool  
34 46. The distal end 48 of the deployment tool 46 can removably attach to the proximal end of the  
35 expandable attachment device 2. The deployment tool 46 can position the expandable attachment



1 device 2 (as shown by arrow in Figure 14). The deployment tool 46 can control radial expansion  
2 68 of each expandable section 30, 32 in unison or independently of one another.

3 [0084] The deployment tool 46, the expandable attachment device 2 or another tool can be used to  
4 create a port 50 into the endoluminal cavity 6 and to ream part or all of the endoluminal cavity 6.

5 [0085] The expandable section 30 can have teeth and/or helical threads 52. The teeth or threads 52  
6 can be configured to anchor to the cortical bone 34 when the expandable section 30 is in a radially  
7 expanded configuration. The expandable attachment device 2 can have an atraumatic tip 26.

8 [0086] Figure 16 illustrates that the first expandable section 36, shown at the distal end 48 of the  
9 expandable attachment device 2 (which is closer to the proximal end of the femur 10) can be  
10 radially expanded first, as shown by arrows. The first expandable section 36 can take on the cross-  
11 section of a circle, square, triangle, oval, or otherwise contour to the shape of the endoluminal  
12 cavity 6 (as shown – see also Figures 27a and 27b), or combinations thereof. The teeth 52 can  
13 engage the cortical bone 34 and anchor the expandable section 30 to the cortical bone 34.

14 [0087] Figure 17 illustrates that the deployment tool 46 can pull, as shown by arrow, the proximal  
15 end of the femur 10 toward the distal end 48 of the femur 10 to close the fracture 14. The force to  
16 pull the proximal end of the femur 10 toward the distal end 48 of the femur 10 can be transmitted  
17 through the unexpandable section 32 and the first expandable section 36 which can be anchored  
18 against the cortical bone 34 of the proximal femur 10. The second expandable section 38 can then  
19 be radially expanded and the deployment tool 46 can be disconnected and removed from the  
20 treatment site (not shown).

21 [0088] Figure 18 illustrates a fracture 14 at the distal end 48 of the femur 10. Figures 19 and 20  
22 illustrate that the one or more fixation screws 54 can be inserted in one or more directions through  
23 the bone 8, and/or across the expandable attachment device 2 and/or the fracture 14. The screws 54  
24 can be inserted through the cells 42 of the expandable section 30. The screws 54 can be sized to be  
25 the same size or smaller than the cells 42 when the expandable section 30 is in a radially contracted  
26 or radially expanded configuration. The cells 42 can be internally threaded to engage the screws 54.  
27 The cells 42, or other holes on the expandable support device can be smaller than, the same size or  
28 larger than the screws diameter. For the cells 42 or holes larger than the screws 54, the screws 54  
29 can slide through the hole during and after deployment.

30 [0089] Figure 21 illustrates that the expandable attachment device 2 can be used for distal radius  
31 72 fracture 14 repair. Additional pins 56 can be placed to secure or control the bone 8 fragments  
32 before, and/or during, and/or after deployment of the expandable attachment device 2. The  
33 expandable attachment device 2 can be straight or have a substantially non-zero radius of curvature  
34 74. The unexpandable sections 32 and/or the expandable sections 30 can be straight or have a  
35 substantially non-zero radius of curvature 74.

1 [0090] Figures 22a through 22c illustrate that the expandable attachment device 2 can be used for  
2 proximal humerus fracture 14 repair.

3 [0091] Figures 23 and 24 illustrate that the device 2 can be inserted and expanded in an  
4 endoluminal cavity 6. Figure 23 illustrates an external view of the insertion and expansion of the  
5 device 2 through the endoluminal channel 6. Figure 24 illustrates that the bone fixation screws 54  
6 can be inserted through (i.e., nested in) the cells 42 of the expandable section 30. The bone fixation  
7 screws 54 can be nested (e.g., pressed against, wedged against) through the cells 42 and/or with the  
8 other bone fixation screws 54.

9 [0092] Figures 25 and 26 illustrate that the expandable attachment device 2 can be deployed in a  
10 phalange 58. For example, the device 2 can be used to treat a broken phalange 58. The  
11 expandable attachment device 2 can be modular. The first expandable section 36 can be removed  
12 from the second expandable section 38. The unexpandable section 32 can have an interlocking  
13 configuration. The physician can construct the expandable attachment device 2 in vivo or in the  
14 operating room before or during deployment, for example, to select the best total length of the  
15 device to insert, and/or to use combinations of expandable sections 30 with different (or the same)  
16 sizes of radial expansion 68.

17 [0093] A traumatic tip 26 (e.g., the screw tip 28) can be covered by an atraumatic tip 26 (e.g., end  
18 cap 60) before or after insertion 62 of the device in the treatment site.

19 [0094] Figures 26a and 26b illustrate that the expandable attachment device 2 can be deployed in  
20 the scaphoid 64. The expandable attachment device 2 can have a proximal anchor 66. The end cap  
21 60 can have a traumatic sharp point, for example, to drive through the bone 8. The proximal anchor  
22 66 can be hit or struck with a hammer or mallet, for example to drive the expandable attachment  
23 device 2 into the scaphoid 64 and/or to radially expand the expandable section 30 (e.g., when the  
24 resistance against the end cap 60 is greater than the force of the hammer, the expandable section 30  
25 can radially expand).

26 [0095] Figures 27a and 27b illustrate that the expandable section 30 of the expandable attachment  
27 device 2 can radially expand to fit the shape of the endoluminal cavity 6. Figure 27a illustrates a  
28 transverse cross-section of the bone 8 with the device 2 inserted into the endoluminal cavity 6.  
29 Figure 27b illustrates that the expandable section 30 can radially expand, as shown by arrows, and  
30 deform to substantially the same shape as the inner wall of the endoluminal cavity 6. The  
31 expandable section 30 can match the interior bone surface contour. For example, this fitting of the  
32 expandable section 30 can increase the anchoring force, torque resistance and healing of the bone  
33 into the expandable section (i.e., through cells of the stent-like expandable section

34 [0096] Figures 28a through 28d illustrate a sequential method for recovering (i.e., removing) the  
35 expandable attachment device 2 from a treatment site. Figure 28a illustrates that the device 2 can  
36 be deployed in a femur, for example extending into the greater trochanter. Figure 28b illustrates

1 that the expandable section **30** can be radially contracted, as shown by arrows. Figure 28c  
2 illustrates that the device **2** can be unscrewed, or otherwise rotated and/or translated, as shown by  
3 arrows, out of the deployment site. Figure 28d illustrates that the endoluminal cavity **6** can remain  
4 in the absence of the device **2**. The endoluminal cavity **6** can be completely or partially filled with  
5 a material listed herein, such as a bone morphogenic protein or morselized bone.

6 **[0097]** Figures 29a through 29d illustrate variations of the distal end **60** of the expandable  
7 attachment device **2** during or after removal from or repositioning in a treatment site. The device **2**  
8 can be removed from a bone in which the device **2** has been deployed and through which bone has  
9 grown.

10 **[0098]** The expandable section **30**, and/or any other hollow section of the device **2** with fluid  
11 communication with the outside of the device **2**, can be more than about 75% filled, for example  
12 about 100% filled with in-grown bone, for example femoral head cancellous bone. The expandable  
13 section **30** and hollows of the device **2** can be packed with bone during or after implantation.  
14 Merely for example, the deployment site can be in or near a trochanter.

15 **[0099]** Figure 29a illustrates that the expandable section **30** of the device **2** can be packed with in-  
16 grown bone when implanted in the target site. Figure 29b illustrates that the expandable section **30**  
17 can be partially radially compressed, as shown by arrows. The packed in-grown bone can exit the  
18 expandable section **30** via the cells in the stent configuration. Figure 29c illustrates that the  
19 expandable section can be further radially compressed, for example returning the radius of the  
20 expandable section **30** to the pre-expansion diameter, and/or an even smaller or a larger diameter  
21 than that of the pre-deployment configuration. Figure 29d illustrates that the expandable support  
22 device **2** can be rinsed and/or otherwise cleaned to remove some or all of the bone extending from  
23 the cells of the expandable section **30**.

24 **[0100]** The device **2** can be withdrawn from and/or repositioned at the target site at any point  
25 during the compression of the expandable section **30** shown in Figures 29a through 29d, but more  
26 force may be needed to withdraw the device **2** when the expandable section **30** is in an expanded  
27 configuration.

28 **[0101]** Figure 30a illustrates that a hollow channel **100** can be defined within the expandable  
29 section **30**. The hollow channel can be packed, as described herein.

30 **[0102]** Figure 30b illustrates that the expandable section **30** can have a bladder or bag **102** attached  
31 to the radially inner surfaces of any or all of the struts **40**. The bag **102** can be an open, closed (e.g.,  
32 contained), or closeable structure. The bag **102** (shown filled) can be filled with any material  
33 disclosed herein, or combinations thereof, for example morselized bone or bone morphogenic  
34 protein. The bag **102** can be porous or non-porous. The bag **102** can be a textile. The bag can  
35 cover all or a portion of the expandable section **30**. The bag **102** can be partially or completely

1 filled (e.g., by feeding, pumping) before, during or after deployment and expansion of the device 2  
2 in the target site.

3 **[0103]** Figure 30c illustrates that the bag 102 can be unattached to the struts 40. For example, the  
4 bag can be loose in the hollow channel 100 or the bag can be attached to the device at one or more  
5 of the longitudinal ends of the hollow channel 100.

6 **[0104]** Figure 30d illustrates that one or more locking rods 104 can be inserted into the expandable  
7 section 30 when the expandable section 30 is in an expanded configuration. The locking rods 104  
8 can be oriented transversely, as shown, and/or longitudinally. The locking rod 104 can be  
9 resiliently attached to one or more struts and deploy automatically when the expandable section 30  
10 is expanded.

11 **[0105]** Figure 31a illustrates that the locking rod 104 can be oriented longitudinally. The locking  
12 rod 104 can have distal attachment elements 106, such as one or more threads, ribs, snaps, brads,  
13 nuts, clips or combinations thereof, at the distal end of the locking rod. The distal attachment  
14 elements 106 can be configured to engagably and releasably attach to one or more distal receiving  
15 elements 108 at the distal end of the device 2, such as one or more threads, ribs, snaps, brads, nuts,  
16 clips, or combinations thereof.

17 **[0106]** The locking rod can have proximal attachment elements 110, such as one or more threads,  
18 ribs, snaps, brads, nuts, clips or combinations thereof, at the proximal end of the locking rod 104.  
19 The proximal attachment elements 110 can be configured to engagably and releasably attach to one  
20 or more proximal receiving elements 112 at the proximal end of the device 2, such as one or more  
21 threads, ribs, snaps, brads, nuts, clips or combinations thereof.

22 **[0107]** The locking rod 104 can fix the length between the distal end and the proximal end of the  
23 expandable portion 30. The distal attachment elements 106 can engage the distal receiving  
24 elements 106 and the proximal attachment elements 108 can engage the proximal receiving  
25 elements 110, for example minimizing and/or substantially eliminating the radial compression and  
26 longitudinal expansion of the expandable section 30.

27 **[0108]** Figure 31b illustrates that the locking rod can have one or more intermediate attachment  
28 elements 114 such as one or more threads, ribs, snaps, brads, nuts, clips or combinations thereof.  
29 The intermediate attachment elements 114 can be located at a position along the locking rod 104  
30 between the distal attachment elements 106 and the proximal attachment elements 110, for  
31 example, such that the intermediate attachment elements 114 can be between the first expandable  
32 section 36 and the second expandable section 38 during use. The intermediate attachment elements  
33 114 can be configured to engagably and releasably attach to one or more intermediate receiving  
34 elements 116 along the device 2 between the first expandable section 36 and the second expandable  
35 section 38. The intermediate receiving elements 116 can be one or more threads, ribs, snaps, brads,  
36 nuts, clips or combinations thereof. The intermediate attachment elements 114 can engage the

1 intermediate receiving elements **116**, for example, minimizing and/or substantially eliminating the  
2 shift of radial expansion to or from the first expandable section **36** from or to, respectively, the  
3 second expandable section **38**.

4 **[0109]** Any or all elements of the device and/or other devices or apparatuses described herein can  
5 be made from, for example, a single or multiple stainless steel alloys, nickel titanium alloys (e.g.,  
6 Nitinol), cobalt-chrome alloys (e.g., ELGILOY® from Elgin Specialty Metals, Elgin, IL;  
7 CONICHROME® from Carpenter Metals Corp., Wyomissing, PA), nickel-cobalt alloys (e.g.,  
8 MP35N® from Magellan Industrial Trading Company, Inc., Westport, CT), molybdenum alloys  
9 (e.g., molybdenum TZM alloy, for example as disclosed in International Pub. No. WO 03/082363  
10 A2, published 9 October 2003, which is herein incorporated by reference in its entirety), tungsten-  
11 rhenium alloys, for example, as disclosed in International Pub. No. WO 03/082363, polymers such  
12 as polyethylene terephthalate (PET), polyester (e.g., DACRON® from E. I. Du Pont de Nemours  
13 and Company, Wilmington, DE), poly ester amide (PEA), polypropylene, aromatic polyesters, such  
14 as liquid crystal polymers (e.g., Vectran, from Kuraray Co., Ltd., Tokyo, Japan), ultra high  
15 molecular weight polyethylene (i.e., extended chain, high-modulus or high-performance  
16 polyethylene) fiber and/or yarn (e.g., SPECTRA® Fiber and SPECTRA® Guard, from Honeywell  
17 International, Inc., Morris Township, NJ, or DYNEEMA® from Royal DSM N.V., Heerlen, the  
18 Netherlands), polytetrafluoroethylene (PTFE), expanded PTFE (ePTFE), polyether ketone (PEK),  
19 polyether ether ketone (PEEK), poly ether ketone ketone (PEKK) (also poly aryl ether ketone  
20 ketone), nylon, polyether-block co-polyamide polymers (e.g., PEBAX® from ATOFINA, Paris,  
21 France), aliphatic polyether polyurethanes (e.g., TECOFLEX® from Thermedics Polymer  
22 Products, Wilmington, MA), polyvinyl chloride (PVC), polyurethane, thermoplastic, fluorinated  
23 ethylene propylene (FEP), absorbable or resorbable polymers such as polyglycolic acid (PGA),  
24 poly-L-glycolic acid (PLGA), polylactic acid (PLA), poly-L-lactic acid (PLLA), polycaprolactone  
25 (PCL), polyethyl acrylate (PEA), polydioxanone (PDS), and pseudo-polyamino tyrosine-based  
26 acids, extruded collagen, silicone, zinc, echogenic, radioactive, radiopaque materials, a biomaterial  
27 (e.g., cadaver tissue, collagen, allograft, autograft, xenograft, bone cement, morselized bone,  
28 osteogenic powder, heads of bone) any of the other materials listed herein or combinations thereof.  
29 Examples of radiopaque materials are barium sulfate, zinc oxide, titanium, stainless steel, nickel-  
30 titanium alloys, tantalum and gold.

31 **[0110]** Any or all elements of the device and/or other devices or apparatuses described herein, can  
32 be, have, and/or be completely or partially coated with agents and/or a matrix a matrix for cell  
33 ingrowth or used with a fabric, for example a covering (not shown) that acts as a matrix for cell  
34 ingrowth. The matrix and/or fabric can be, for example, polyester (e.g., DACRON® from E. I. Du  
35 Pont de Nemours and Company, Wilmington, DE), poly ester amide (PEA), polypropylene, PTFE,  
36 ePTFE, nylon, extruded collagen, silicone, any other material disclosed herein, or combinations  
37 thereof.

1 [0111] The device and/or elements of the device and/or other devices or apparatuses described  
2 herein and/or the fabric can be filled, coated, layered and/or otherwise made with and/or from  
3 cements, fillers, glues, and/or an agent delivery matrix known to one having ordinary skill in the art  
4 and/or a therapeutic and/or diagnostic agent. Any of these cements and/or fillers and/or glues can  
5 be osteogenic and osteoinductive growth factors.

6 [0112] Examples of such cements and/or fillers includes bone chips, demineralized bone matrix  
7 (DBM), calcium sulfate, coralline hydroxyapatite, biocoral, tricalcium phosphate, calcium  
8 phosphate, polymethyl methacrylate (PMMA), biodegradable ceramics, bioactive glasses,  
9 hyaluronic acid, lactoferrin, bone morphogenic proteins (BMPs) such as recombinant human bone  
10 morphogenetic proteins (rhBMPs), other materials described herein, or combinations thereof.

11 [0113] The agents within these matrices can include any agent disclosed herein or combinations  
12 thereof, including radioactive materials; radiopaque materials; cytogenic agents; cytotoxic agents;  
13 cytostatic agents; thrombogenic agents, for example polyurethane, cellulose acetate polymer mixed  
14 with bismuth trioxide, and ethylene vinyl alcohol; lubricious, hydrophilic materials; phosphor  
15 cholene; anti-inflammatory agents, for example non-steroidal anti-inflammatories (NSAIDs) such  
16 as cyclooxygenase-1 (COX-1) inhibitors (e.g., acetylsalicylic acid, for example ASPIRIN® from  
17 Bayer AG, Leverkusen, Germany; ibuprofen, for example ADVIL® from Wyeth, Collegeville, PA;  
18 indomethacin; mefenamic acid), COX-2 inhibitors (e.g., VIOXX® from Merck & Co., Inc.,  
19 Whitehouse Station, NJ; CELEBREX® from Pharmacia Corp., Peapack, NJ; COX-1 inhibitors);  
20 immunosuppressive agents, for example Sirolimus (RAPAMUNE®, from Wyeth, Collegeville,  
21 PA), or matrix metalloproteinase (MMP) inhibitors (e.g., tetracycline and tetracycline derivatives)  
22 that act early within the pathways of an inflammatory response. Examples of other agents are  
23 provided in Walton et al, Inhibition of Prostaglandin E<sub>2</sub> Synthesis in Abdominal Aortic Aneurysms,  
24 *Circulation*, July 6, 1999, 48-54; Tambiah et al, Provocation of Experimental Aortic Inflammation  
25 Mediators and Chlamydia Pneumoniae, *Brit. J. Surgery* 88 (7), 935-940; Franklin et al, Uptake of  
26 Tetracycline by Aortic Aneurysm Wall and Its Effect on Inflammation and Proteolysis, *Brit. J.*  
27 *Surgery* 86 (6), 771-775; Xu et al, Sp1 Increases Expression of Cyclooxygenase-2 in Hypoxic  
28 Vascular Endothelium, *J. Biological Chemistry* 275 (32) 24583-24589; and Pyo et al, Targeted  
29 Gene Disruption of Matrix Metalloproteinase-9 (Gelatinase B) Suppresses Development of  
30 Experimental Abdominal Aortic Aneurysms, *J. Clinical Investigation* 105 (11), 1641-1649 which  
31 are all incorporated by reference in their entireties.

32 [0114] Other examples of fractures types that can be treated with the disclosed device and method  
33 include Greenstick fractures, transverse fractures, fractures across growth plates, simple fractures,  
34 wedge fractures, complex fractures, compound fractures, complete fractures, incomplete fractures,  
35 linear fractures, spiral fractures, transverse fractures, oblique fractures, comminuted fractures,  
36 impacted fractures, and soft tissue tears, separations (e.g., avulsion fracture), sprains, and

1 combinations thereof. Plastic deformations of bones can also be treated with the disclosed device  
2 and method.

3 **[0115]** Other examples of bones that can be treated with the disclosed device and method include  
4 the fingers (e.g., phalanges), hands (e.g., metacarpals, carpus), toes (e.g., tarsals), feet (metatarsals,  
5 tarsus), legs(e.g., femur, tibia, fibula), arms (e.g., humerus, radius, ulna), scapula, coccyx, pelvis,  
6 clavicle, scapula, patella, sternum, ribs, or combinations thereof. For example, the device can be  
7 used in the femoral neck, femoral shaft, proximal or distal tibia or the shaft of the tibia, the  
8 humerus, the forearm, the ankle, small bones, the clavicle, and for revision surgery, such as hoip  
9 revision surgery.

10 **[0116]** Any elements described herein as singular can be pluralized (i.e., anything described as  
11 “one” can be more than one). Any species element of a genus element can have the characteristics  
12 or elements of any other species element of that genus. The above-described configurations,  
13 elements or complete assemblies and methods and their elements for carrying out the invention, and  
14 variations of aspects of the invention can be combined and modified with each other in any  
15 combination.

## CLAIMS

1 We Claim:

2 1. A method for repairing a bone fracture comprising:

3       inserting into an endoluminal channel a device having a first radially expandable portion  
4 and a second radially expandable portion, wherein the device has an unexpandable length between  
5 the first radially expandable portion and the second radially expandable portion..  
6

7  
8 2. The method of Claim 1, further comprising positioning the first radially expandable portion on a  
9 first side of the fracture.

10  
11 3. The method of Claim 2, further comprising positioning the second radially expandable portion  
12 on a second side of the fracture.

13  
14 4. The method of Claim 3, further comprising radially expanding the first radially expandable  
15 portion.

16  
17 5. The method of Claim 4, further comprising radially expanding the second radially expandable  
18 portion.

19  
20 6. The method of Claim 1, further comprising radially expanding the first radially expandable  
21 portion.

22  
23 7. The method of Claim 6, further comprising radially expanding the second radially expandable  
24 portion.

25  
26 8. The method of Claim 1, further comprising inserting a fixation device through the bone and the  
27 first radially expandable portion.

28  
29 9. The method of Claim 5, further comprising inserting a fixation device through the bone and the  
30 first radially expandable portion.

31 10. The method of Claim 6, wherein radially expanding the first radially expandable portion  
32 comprises deforming the first radially expandable portion to substantially fit an inner contour of the  
33 endoluminal channel.

34  
35 11. The method of Claim 6, further comprising radially contracting the first radially expandable  
36 portion, and further comprising repositioning the device in the endoluminal channel or removing  
37 the device from the endoluminal channel.



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12. The method of Claim 6, wherein the first radially expandable portion is substantially hollow, and further comprising filling the first radially expandable portion with a filler.

13. The method of Claim 12, wherein the filler comprises bone.

14. The method of Claim 12, wherein the filler comprises a protein.

15. The method of Claim 12, wherein filling comprises filling into a contained bladder.

16. The method of Claim 6, further comprising locking the first radially expandable portion in an expanded configuration.

17. A method for repairing a bone fracture comprising:  
inserting into an endoluminal channel a device having a first radially expandable portion and a second radially expandable portion.

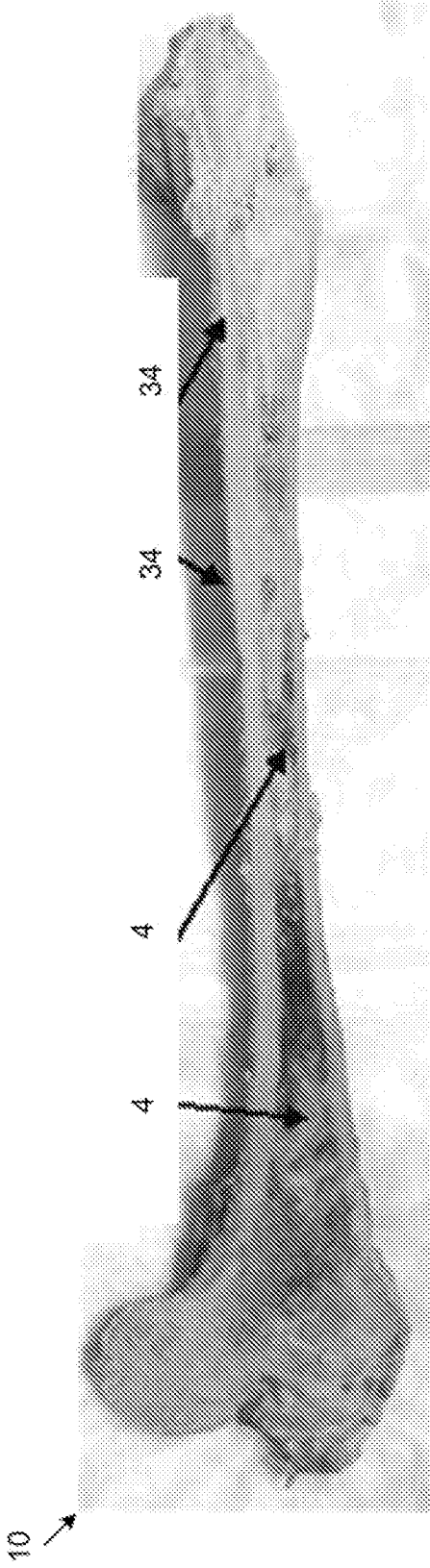
18. The method of Claim 17, further comprising radially expanding the first radially expandable portion and the second radially expandable portion.

19. The method of Claim 18, wherein inserting comprises screwing the device into the bone.

20. A method for repairing a bone fracture comprising:  
inserting into an endoluminal channel a support element having a first radially expandable portion at a first length along the support element and wherein the expandable portion defines a hollow channel,  
radially expanding the first radially expandable portion,  
inserting a locking rod into the hollow channel, and  
attaching the locking rod to the support element distal and proximal to the first radially expandable portion.

21. The method of Claim 20, further comprising filling the hollow channel with a filler.

22. the method of Claim 20, wherein the support element has a second radially expandable portion at a second length along the support element, the method further comprising radially expanding the second radially expandable portion, and attaching the locking rod to the support element distal and proximal to the second radially expandable portion.



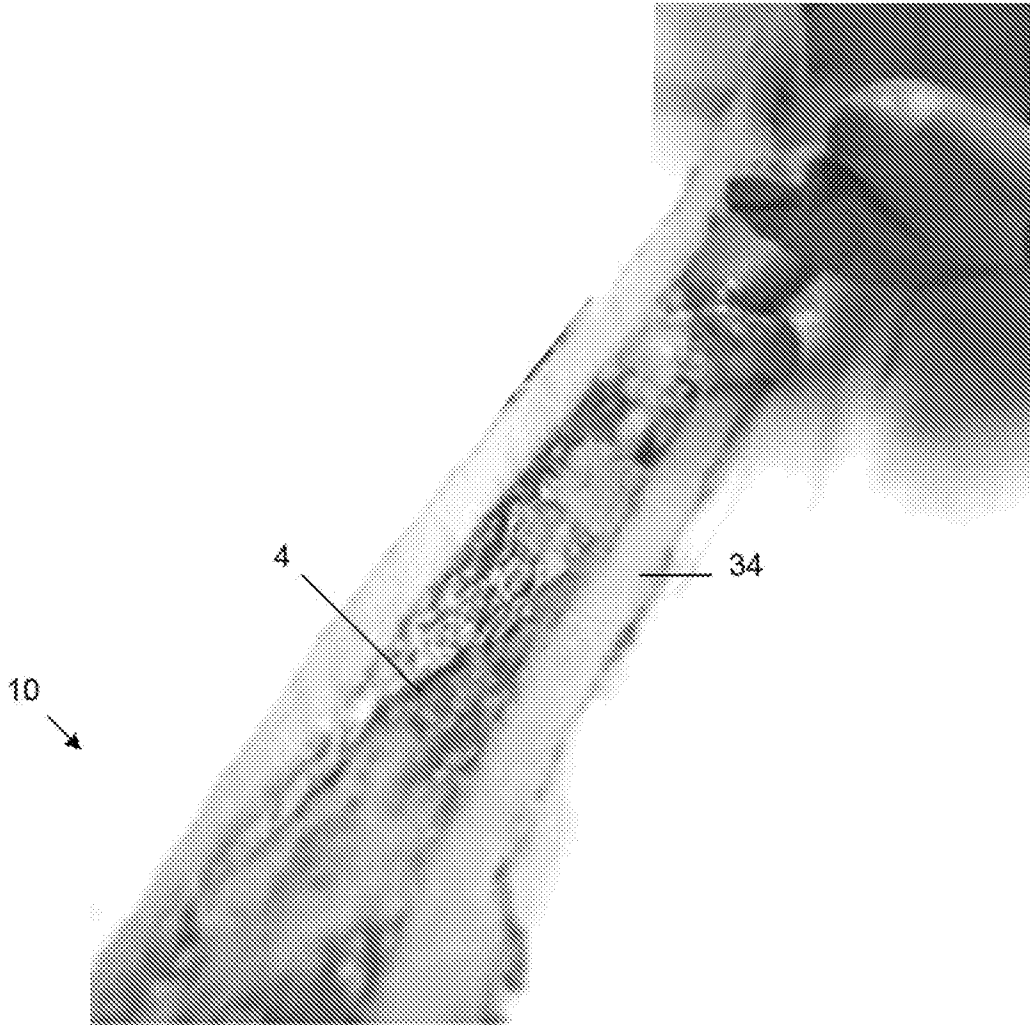
NOT INVENTION

Fig. 1

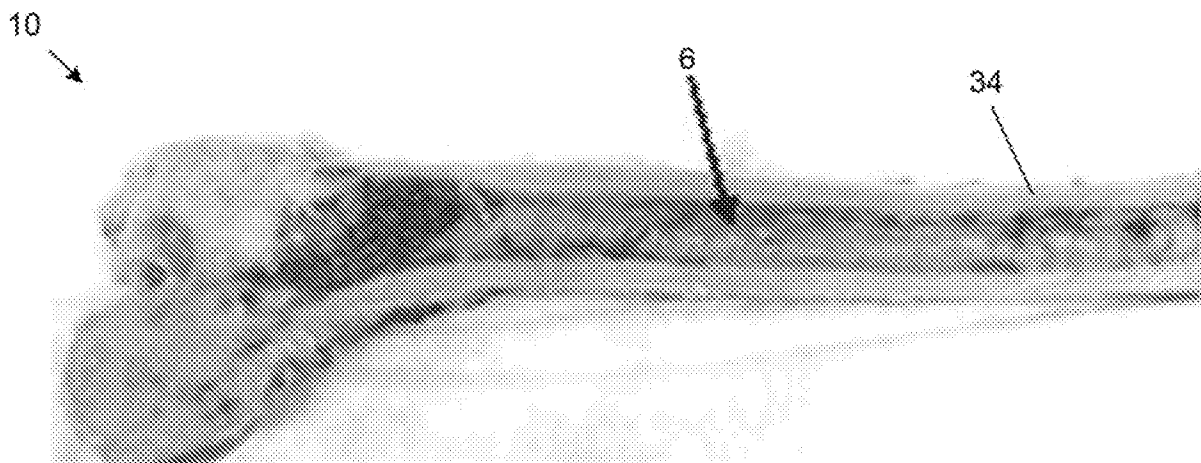


NOT INVENTION

Fig. 2



NOT INVENTION  
Fig. 3



NOT INVENTION  
Fig. 4

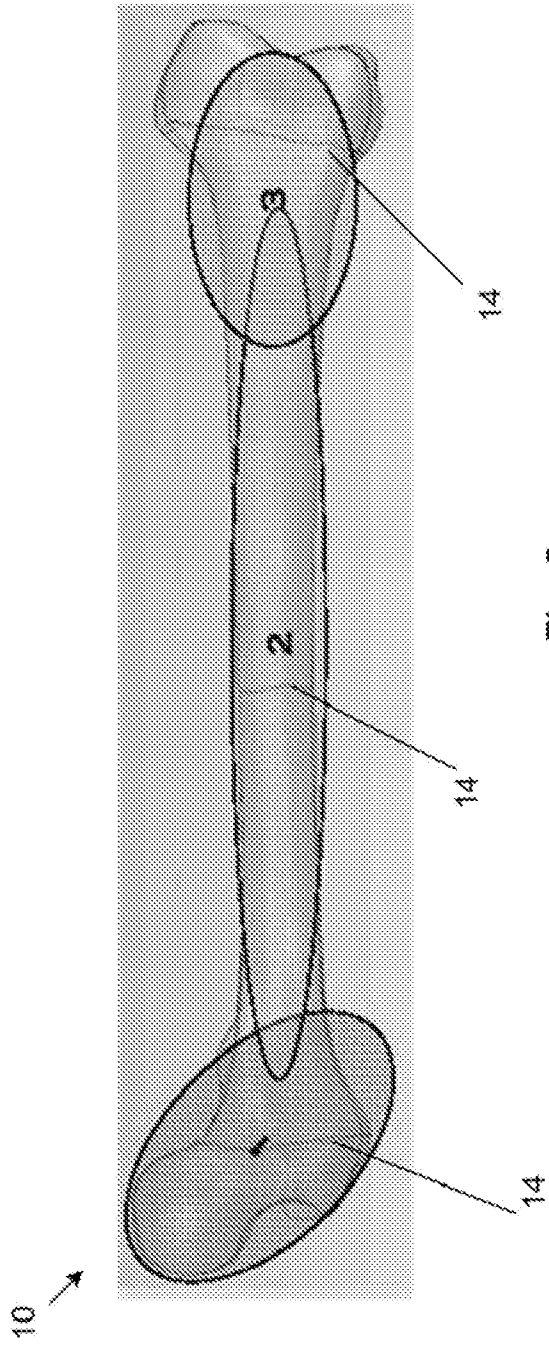


Fig. 5

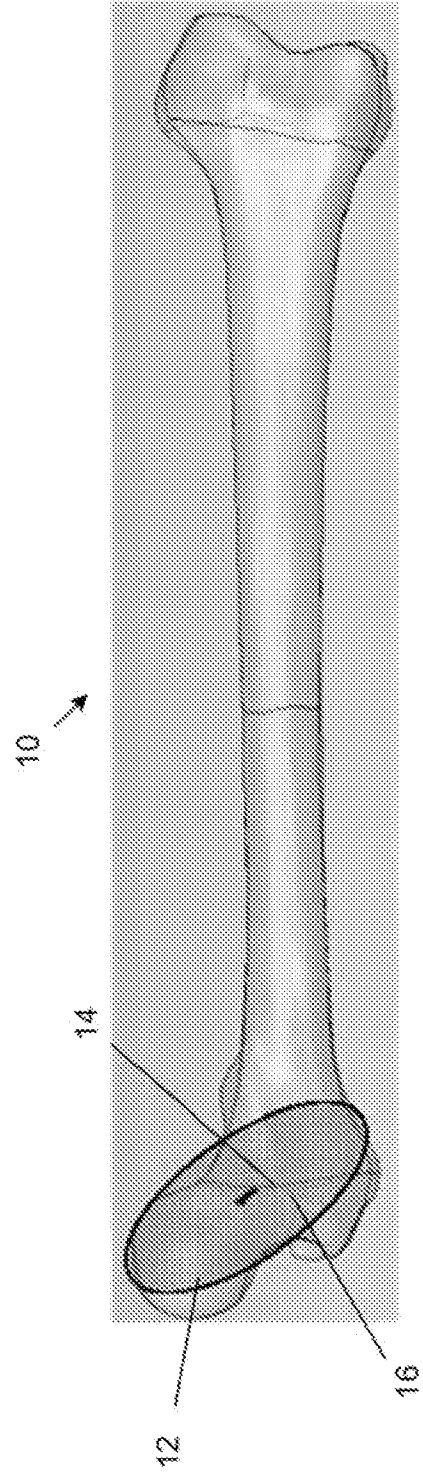


Fig. 6

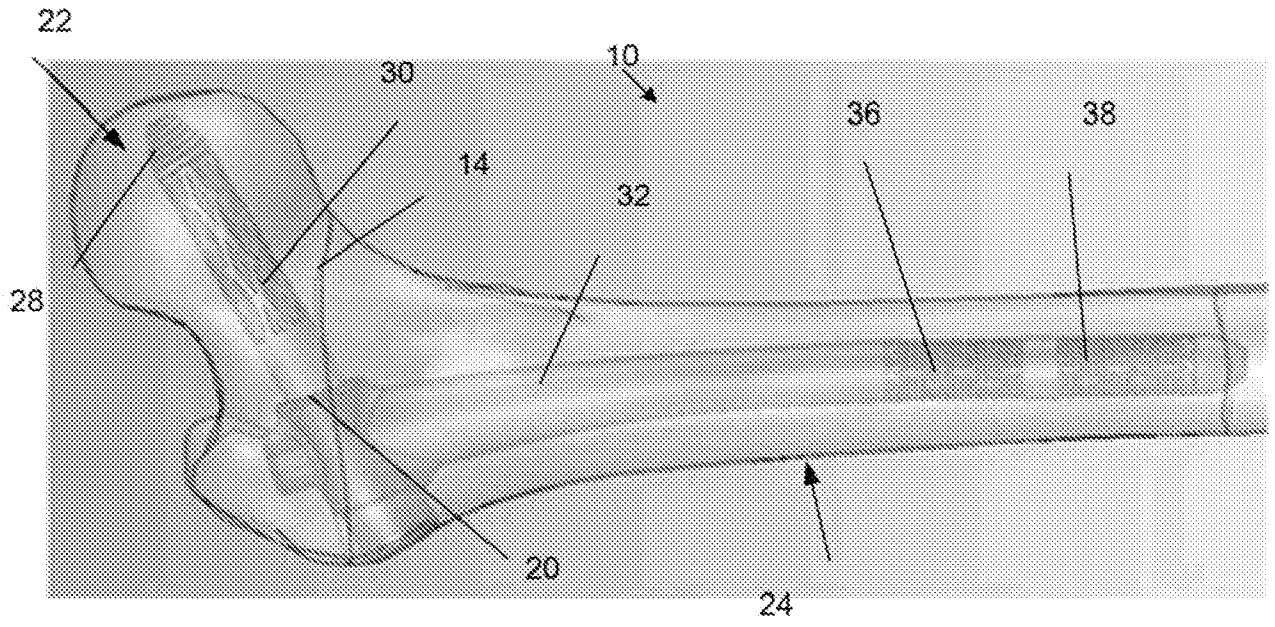


Fig. 7

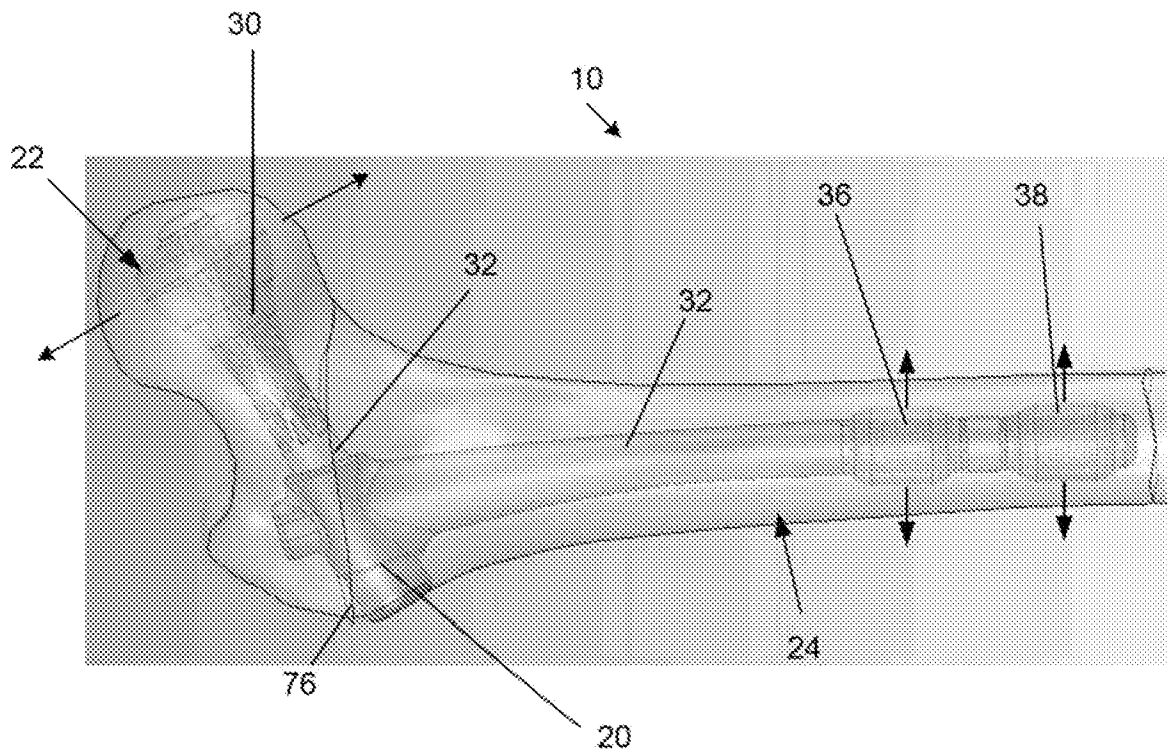


Fig. 8

Fig. 9a

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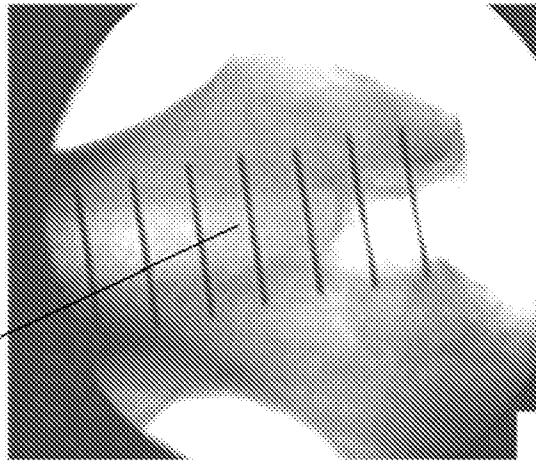


Fig. 9b

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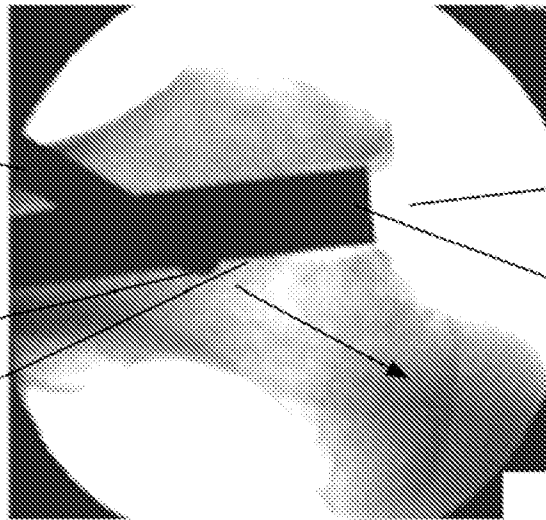


Fig. 9c

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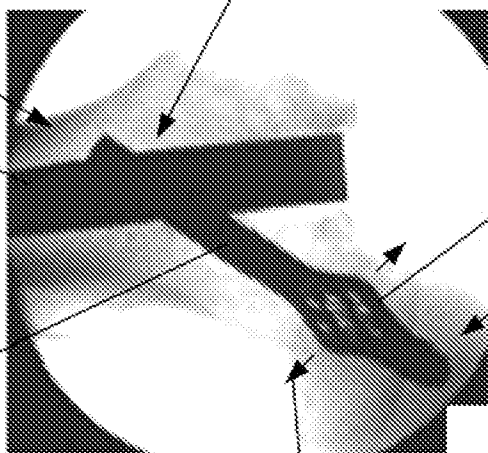
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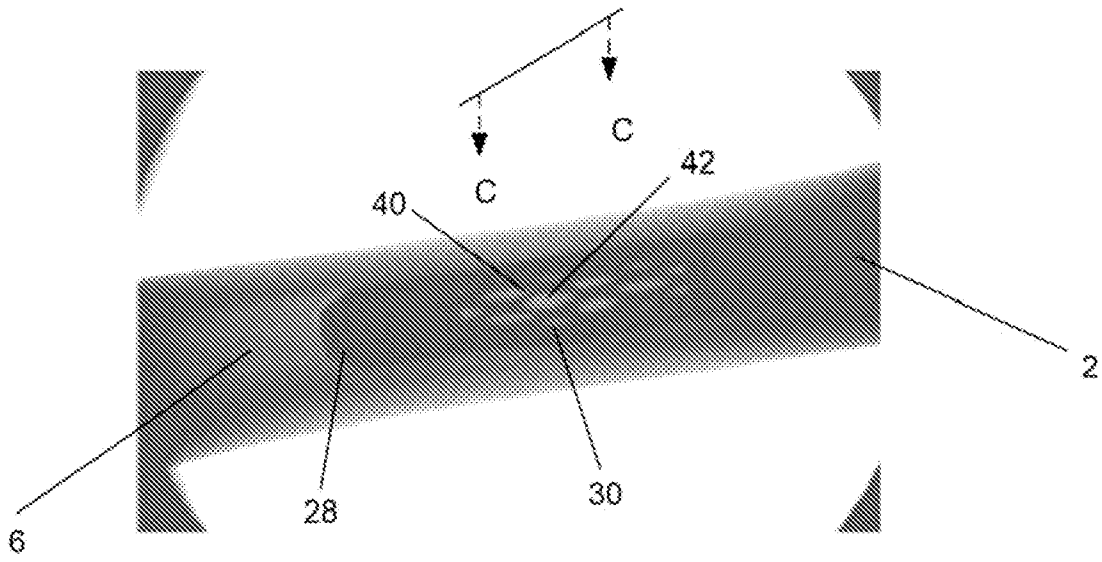


Fig. 10a

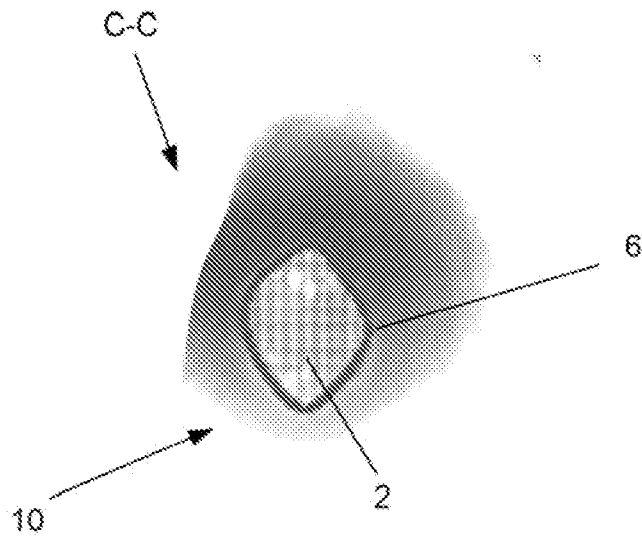
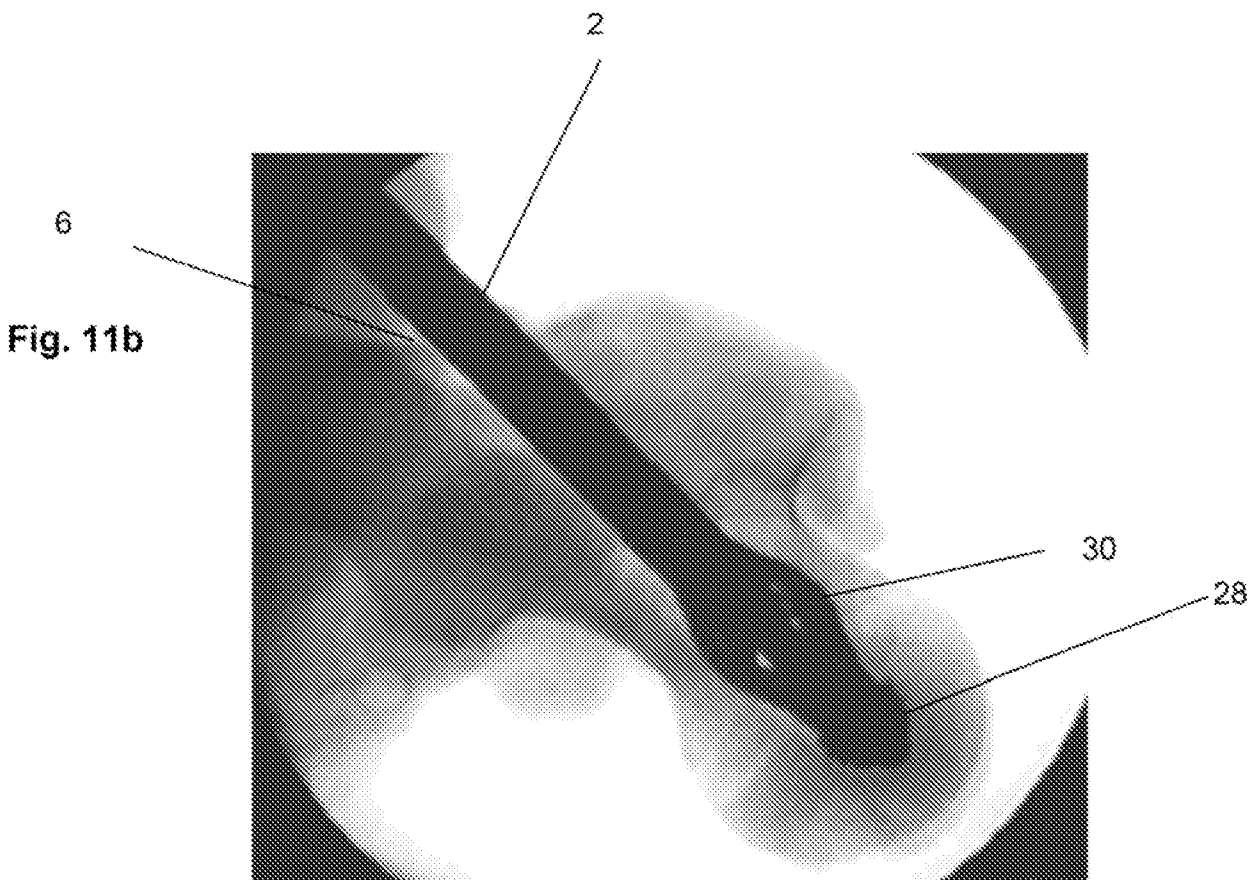
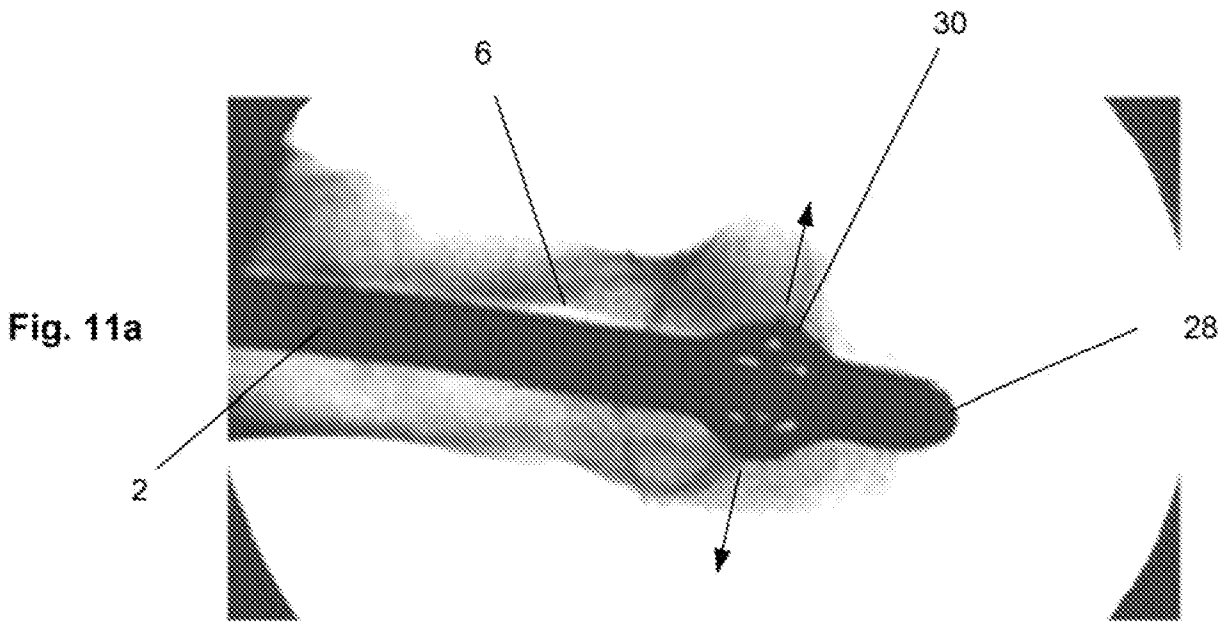


Fig. 10b





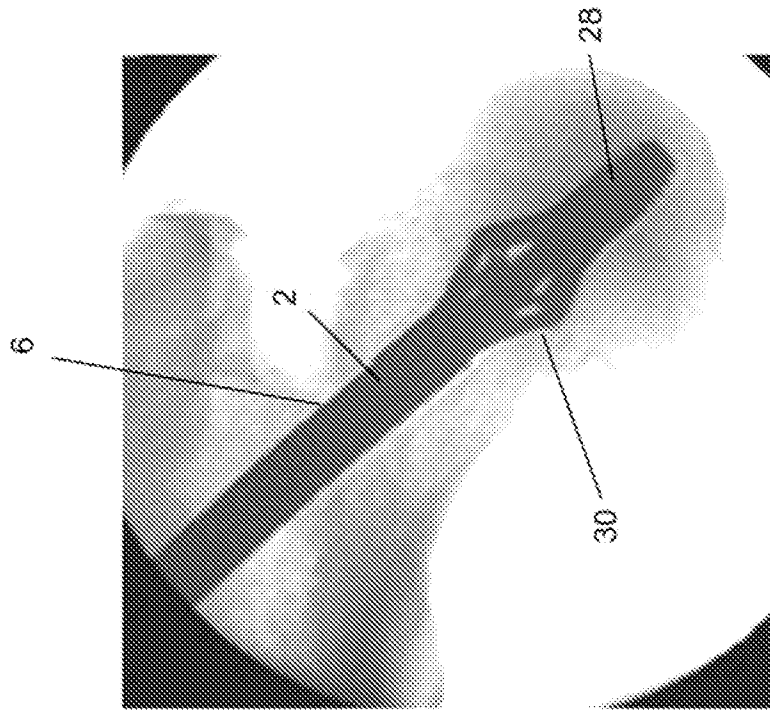


Fig. 12b

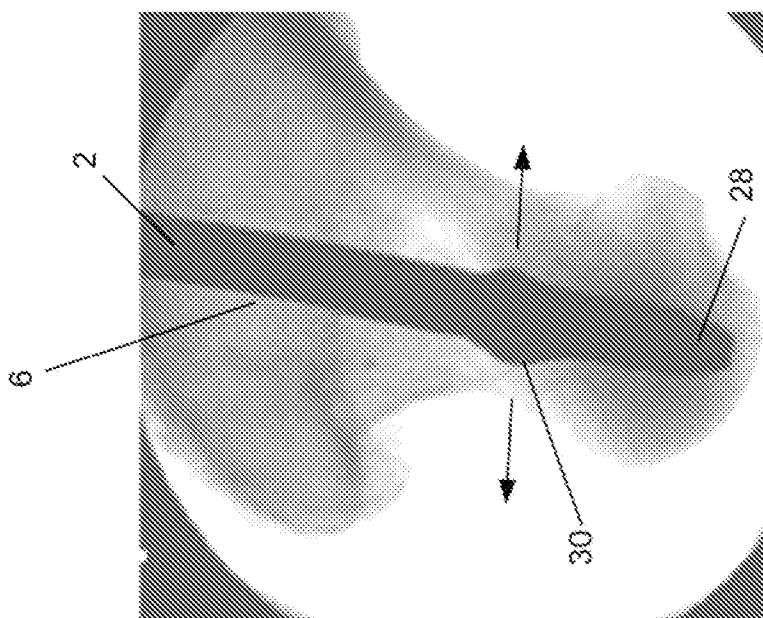


Fig. 12a

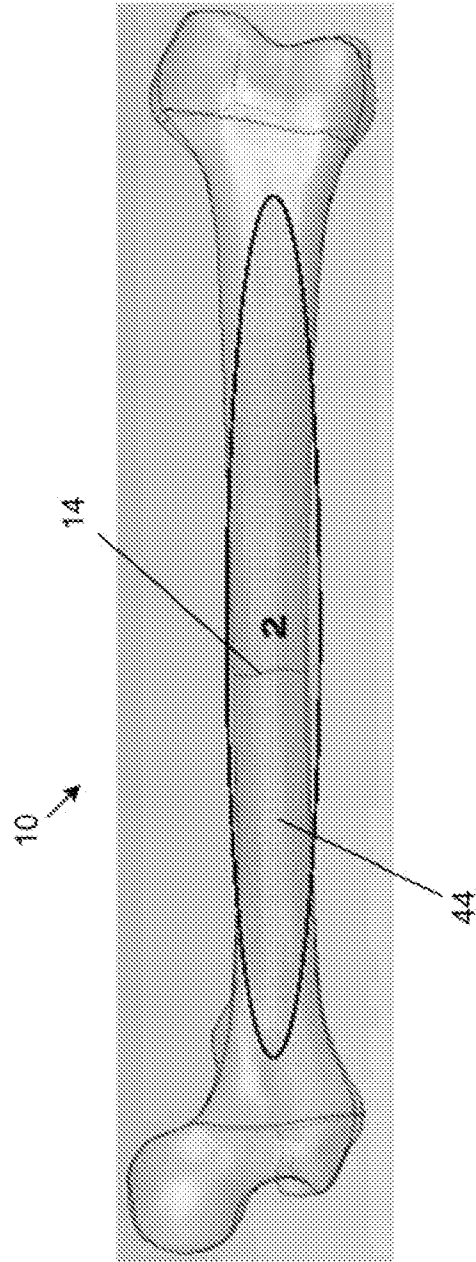


Fig. 13

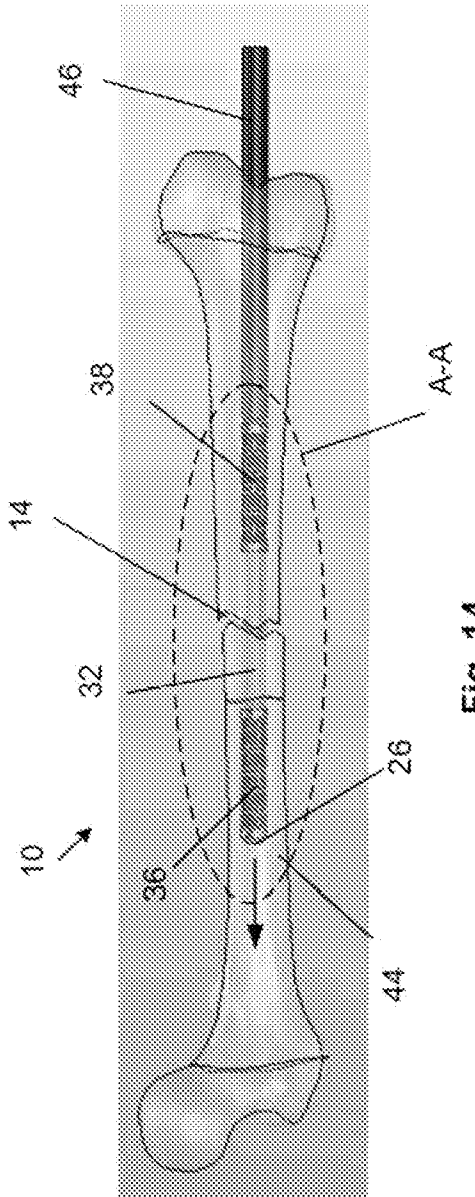


Fig. 14

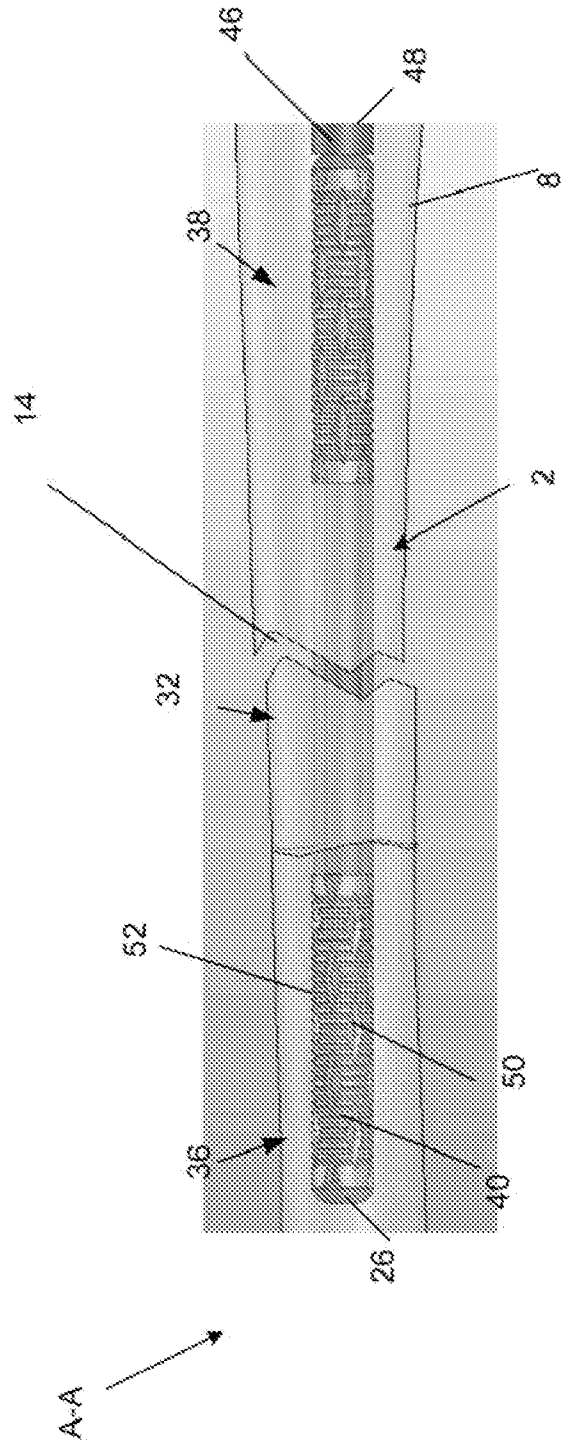


Fig. 15

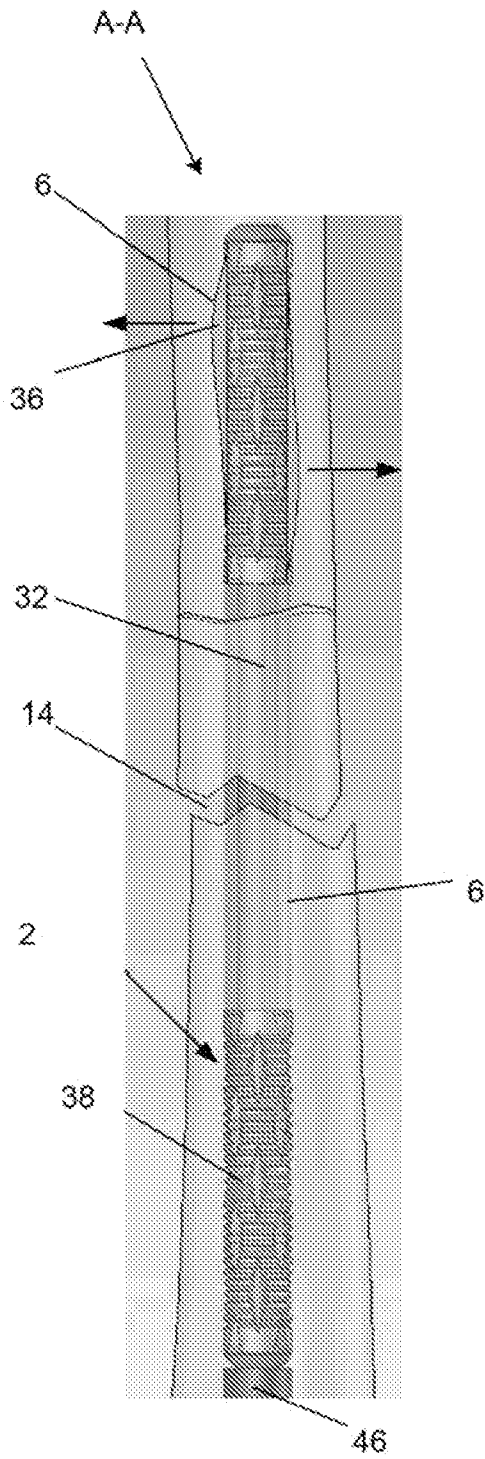


Fig. 16

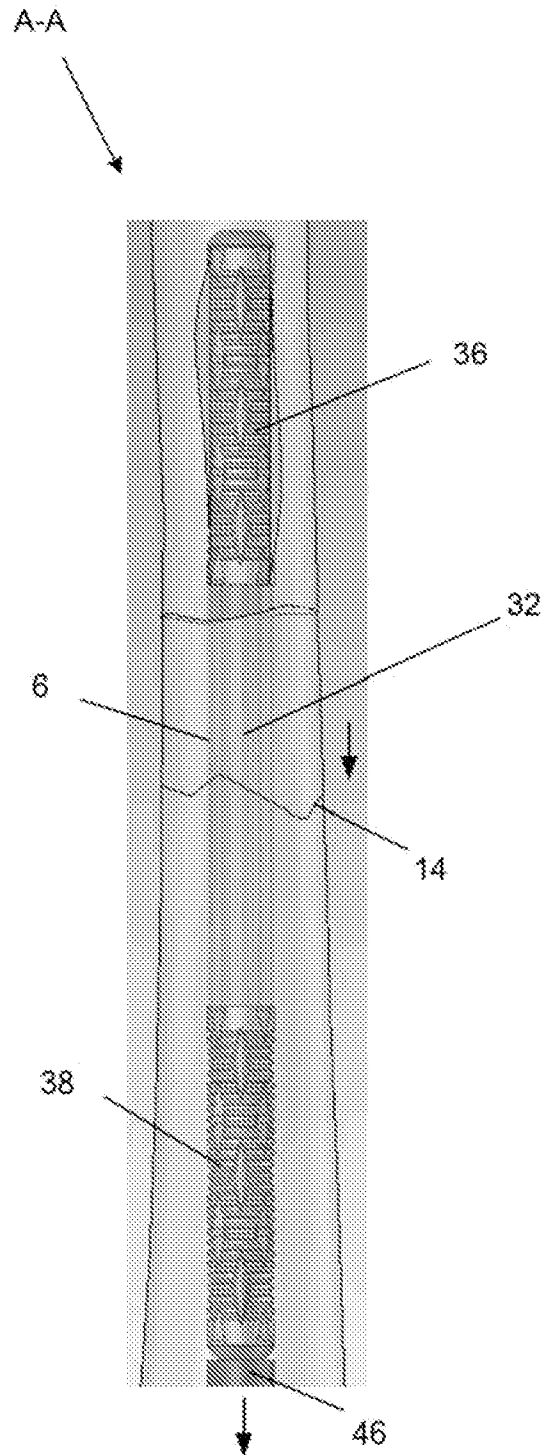


Fig. 17

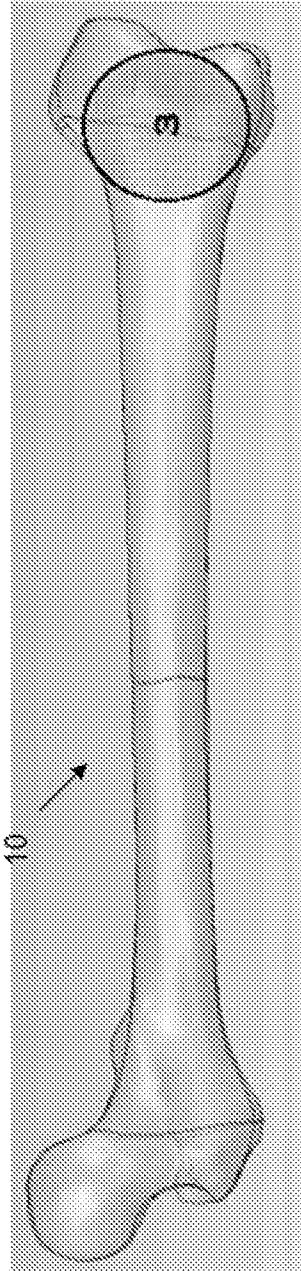


Fig. 18

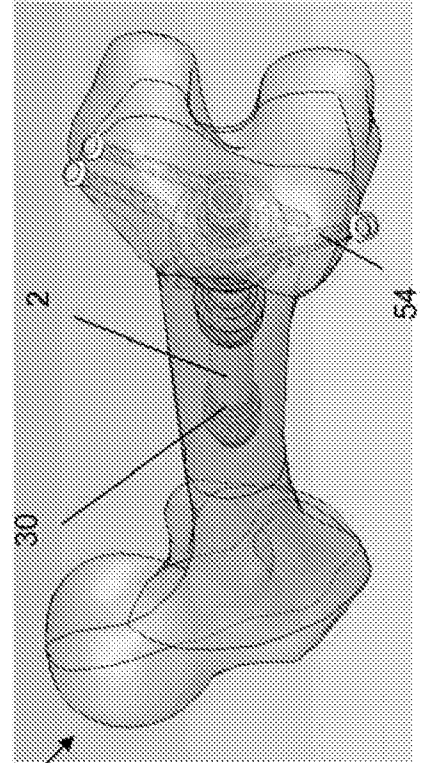
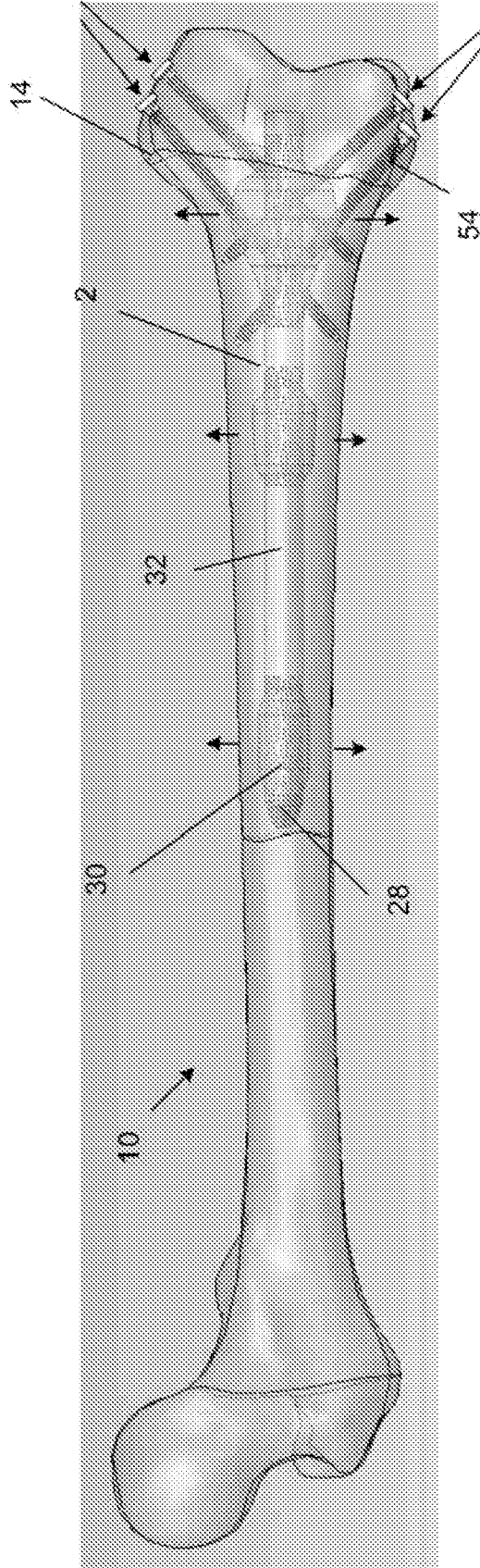


Fig. 19

Fig. 20

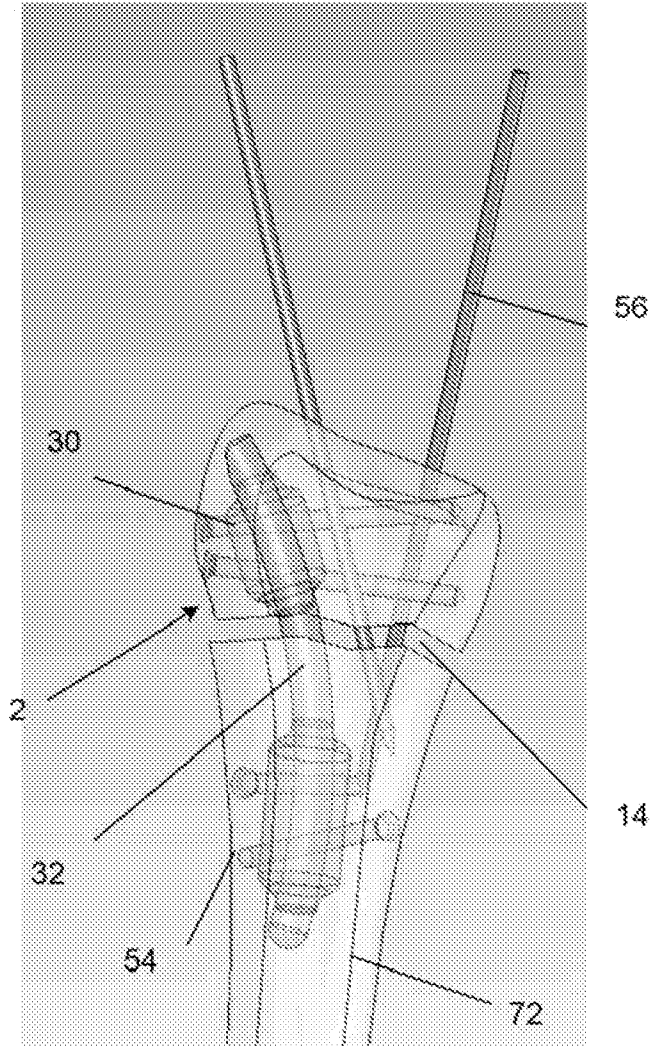


Fig. 21

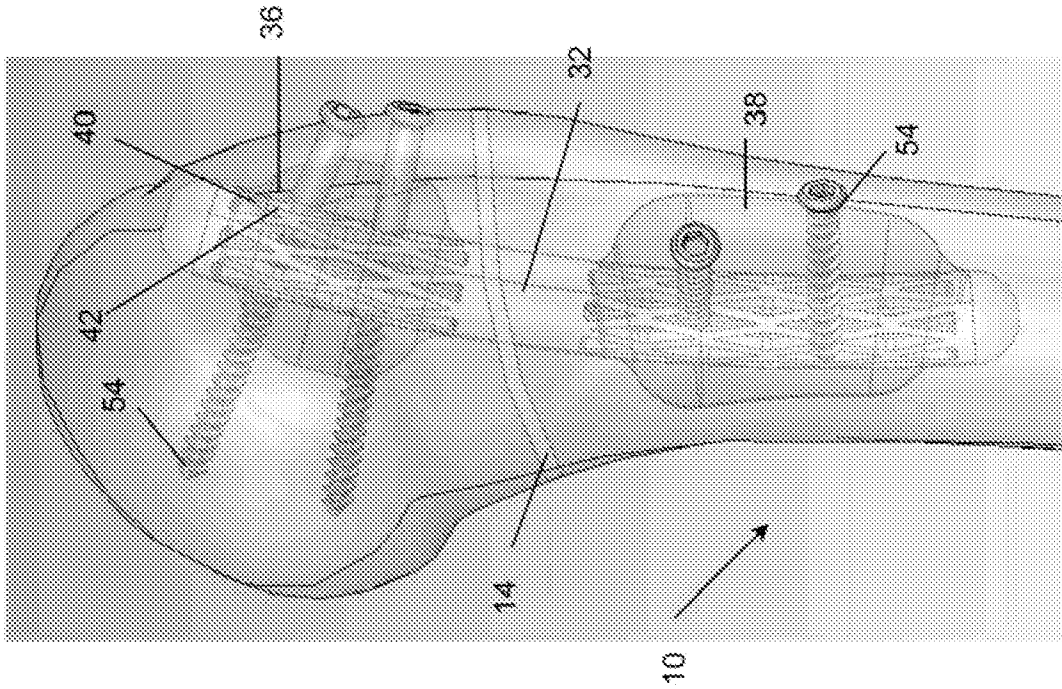


Fig. 22c

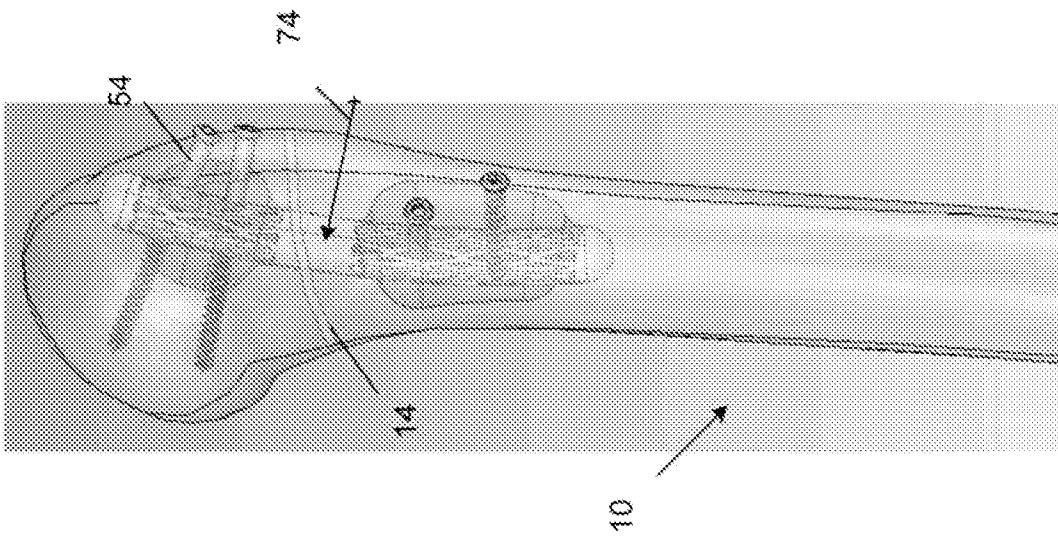


Fig. 22b

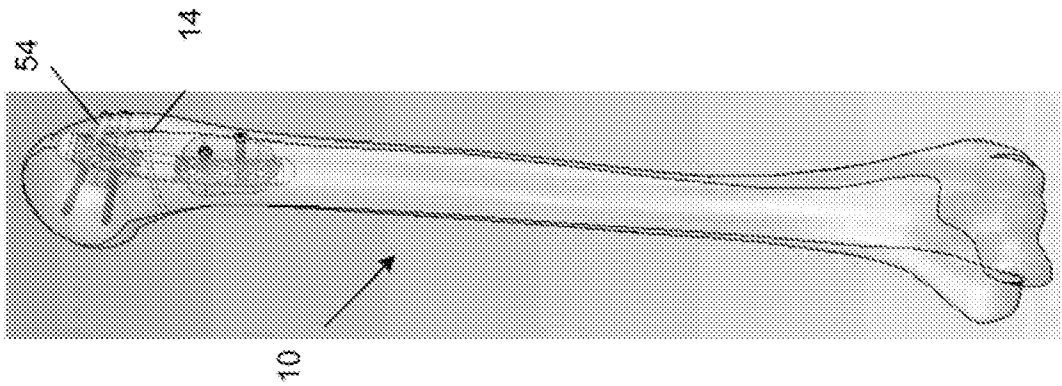


Fig. 22a

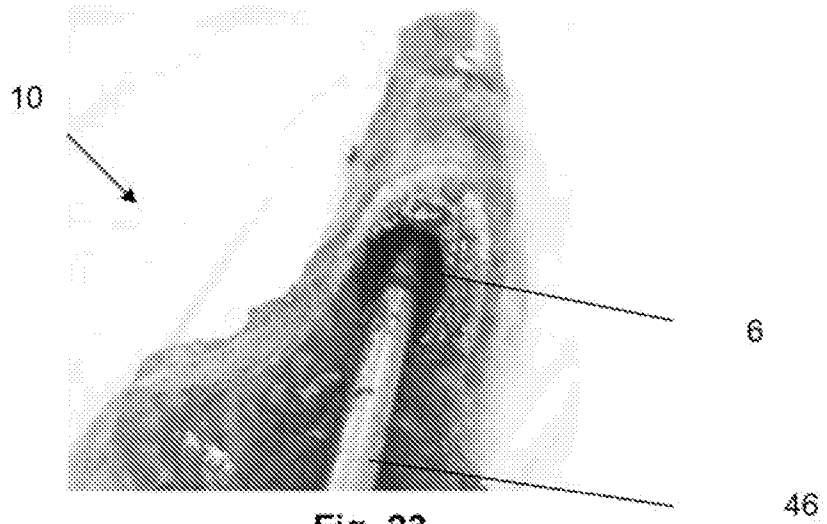


Fig. 23

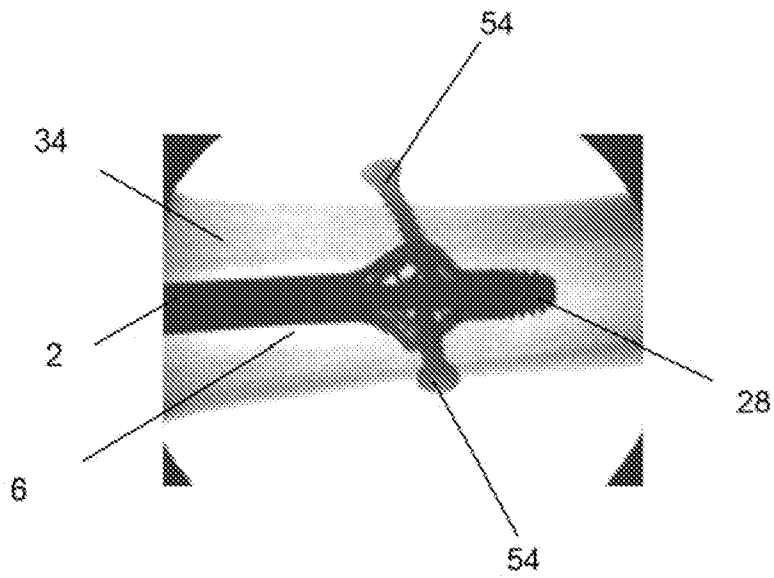
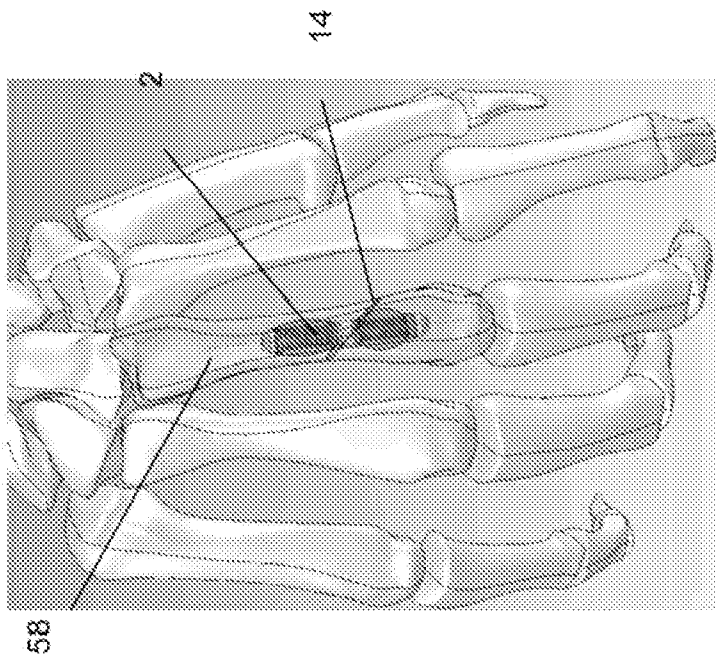
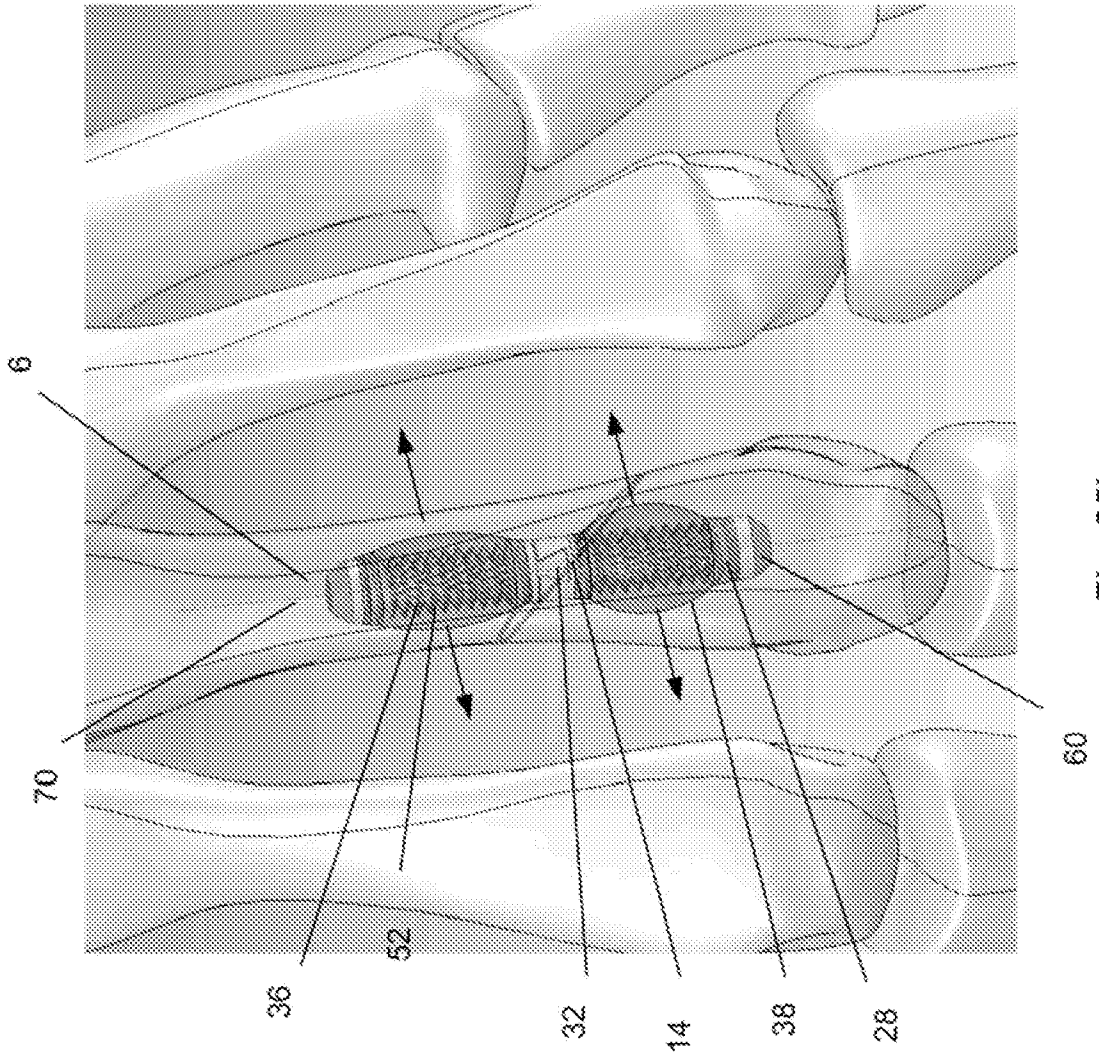


Fig. 24





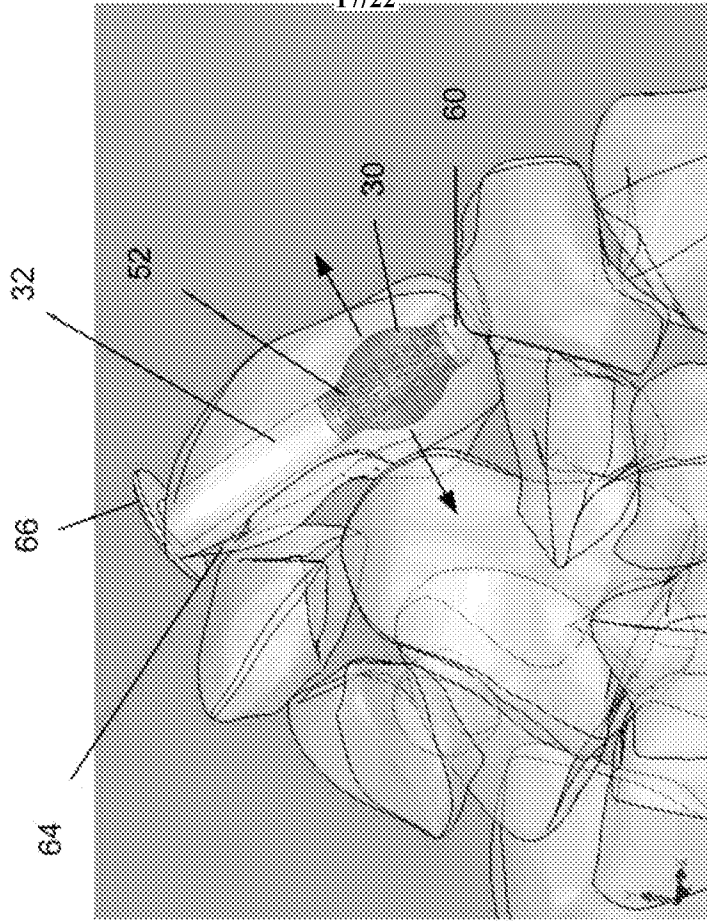


Fig. 26b

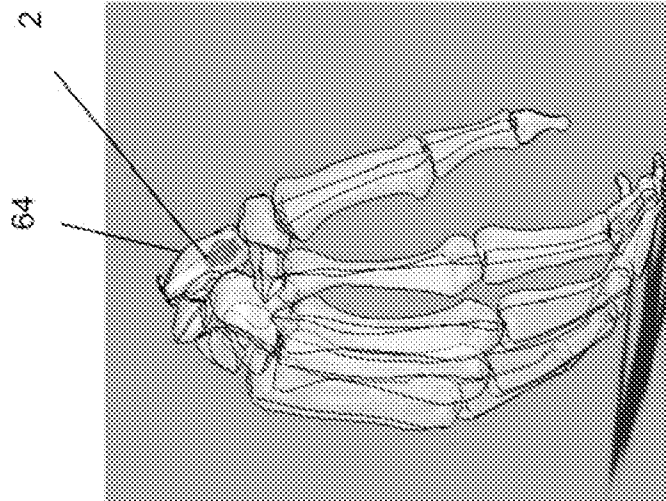


Fig. 26a

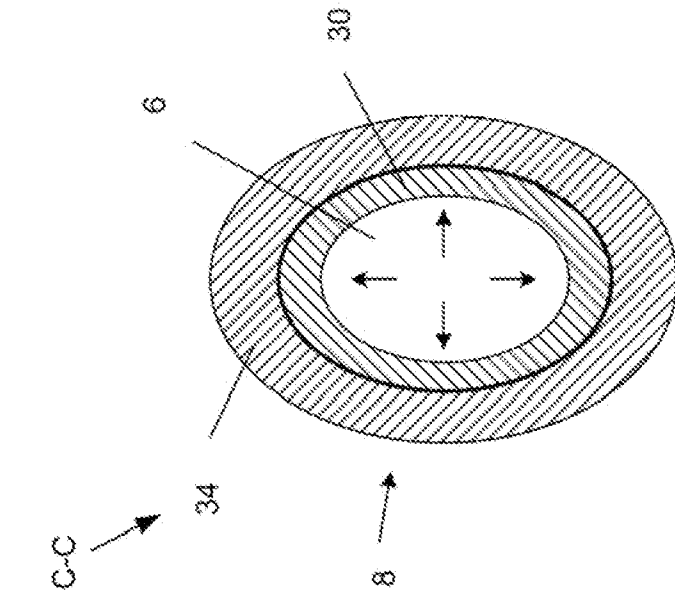


Fig. 27b

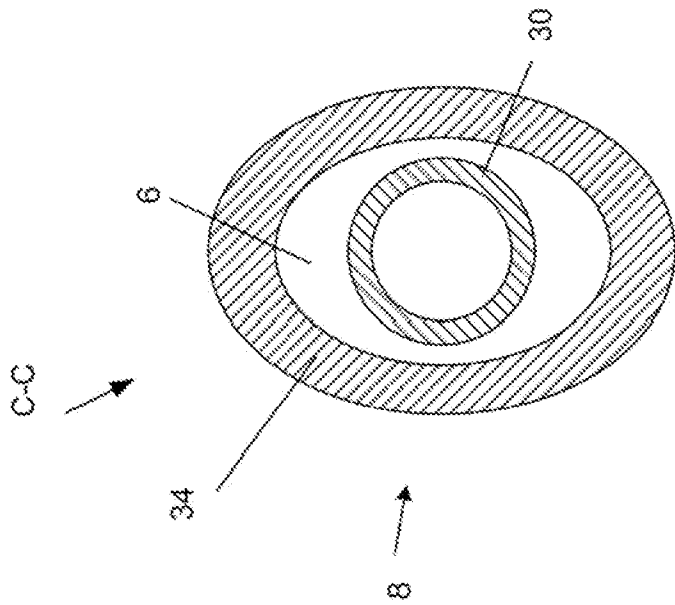


Fig. 27a

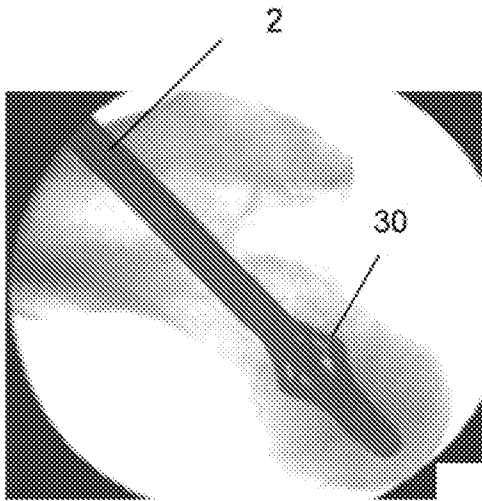


Fig. 28a

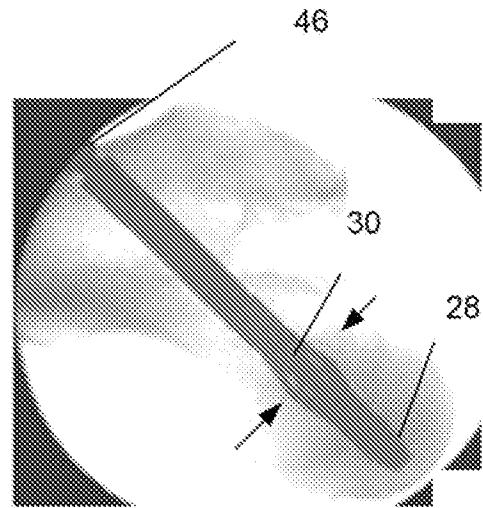


Fig. 28b

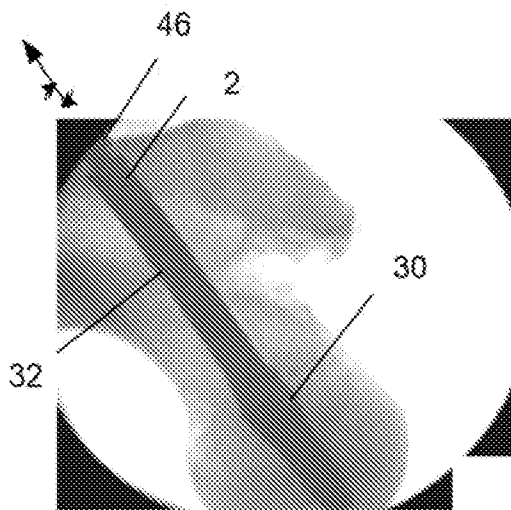


Fig. 28c

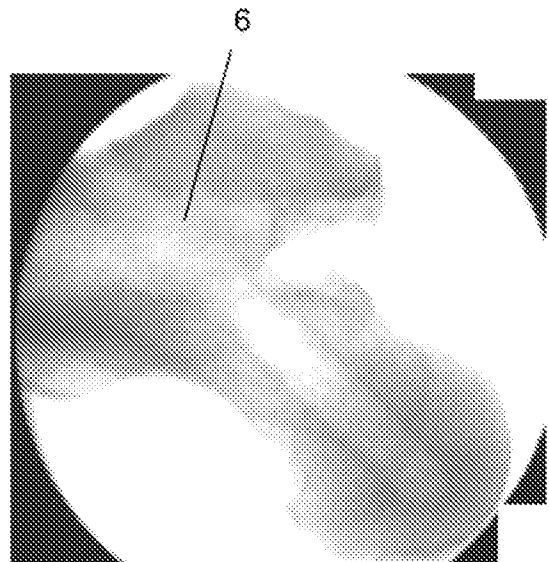


Fig. 28d

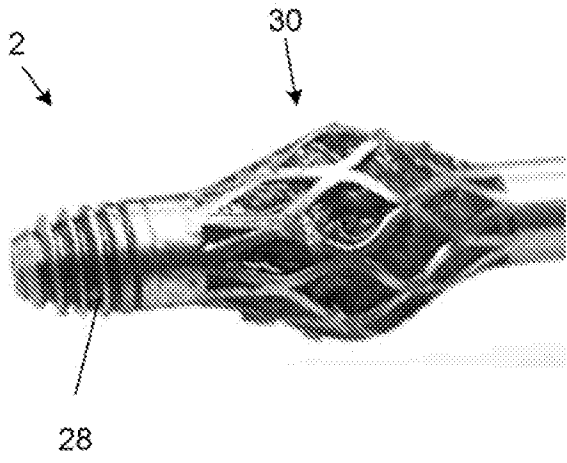


Fig. 29a

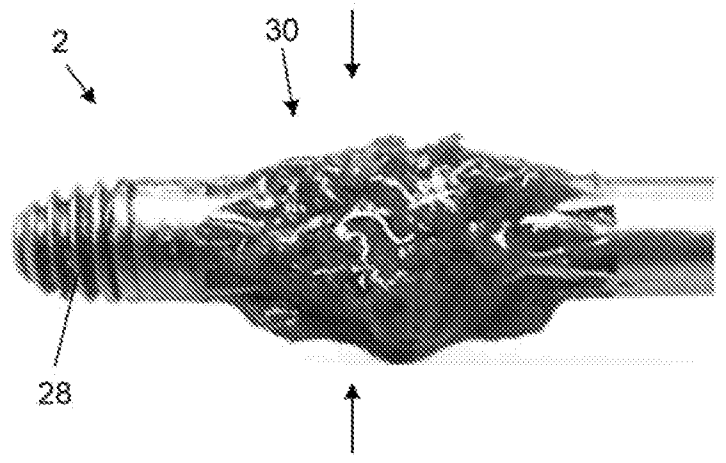


Fig. 29b

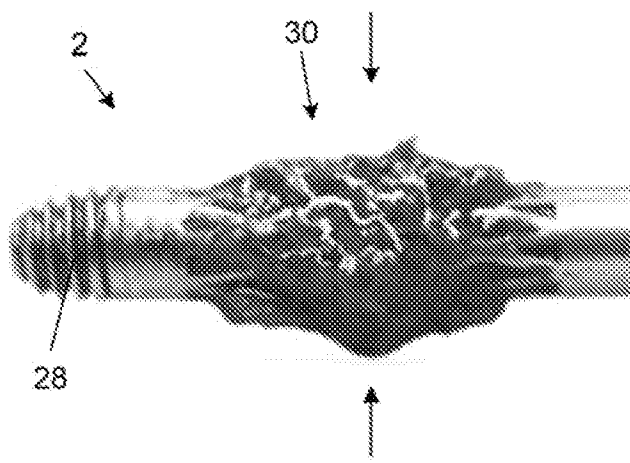


Fig. 29c

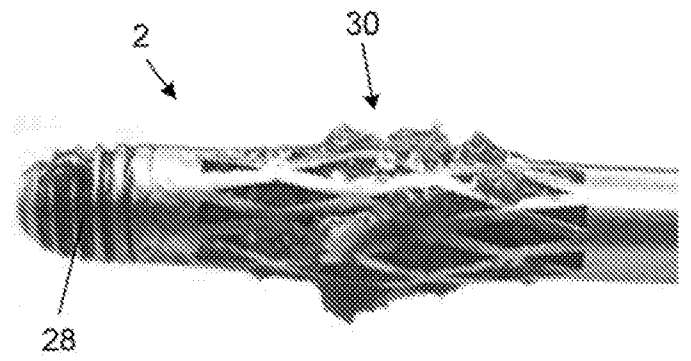


Fig. 29d

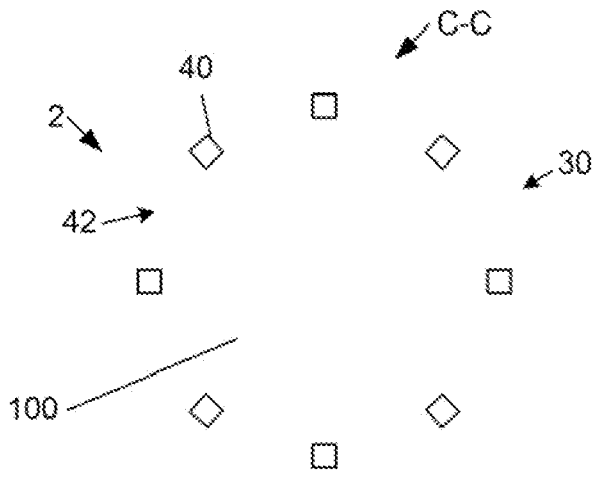


Fig. 30a

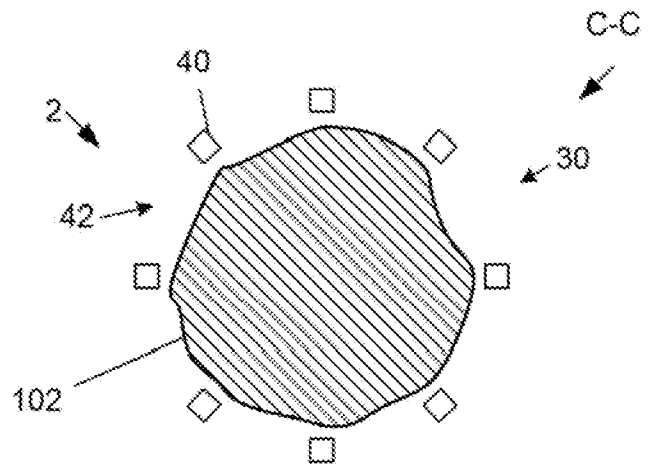


Fig. 30c

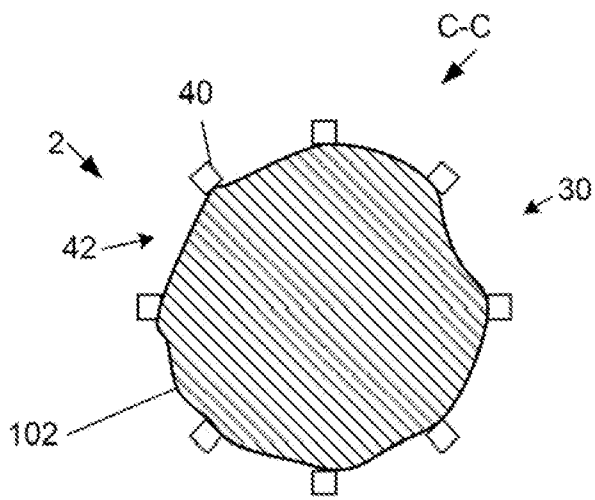


Fig. 30b

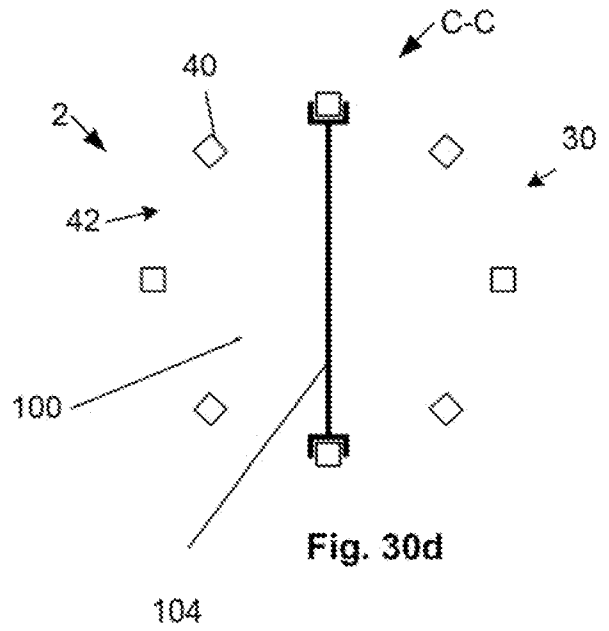


Fig. 30d

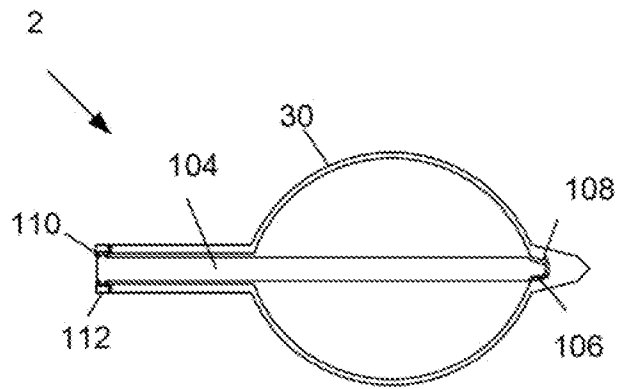


Fig. 31a

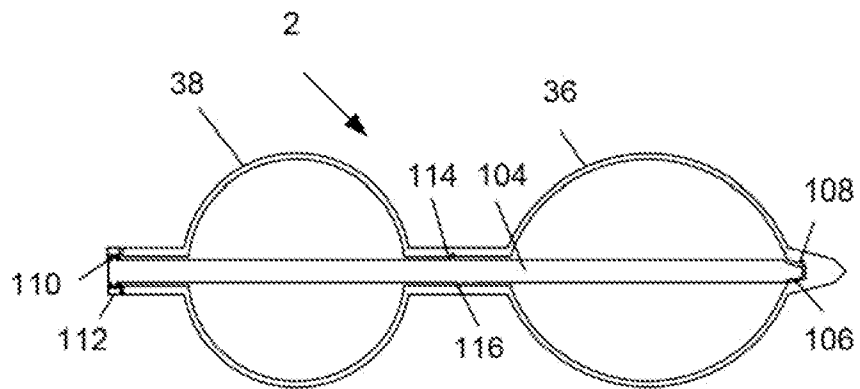


Fig. 31b

**INTERNATIONAL SEARCH REPORT**

International application No.  
PCT/US 09/31727

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC(8) - A61B 17/58, A61B 17/60, A61F 2/00 (2009.01)  
USPC - 606/105  
According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)  
IPC (8) - A61B 17/58, A61B 17/60, A61F 2/00 (2009.01)  
USPC - 606/105

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched  
USPC - 606/53, 60, 62, 63, 64, 86R; 623/11.11, 16.11, 23.47 - see keywords below

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)  
PubWEST (USPT, PGPB, EPAB, JPAB); Google Scholar - Bone, fracture, endoluminal channel, radially, expandable, Greenhalgh, Romano, repair, medullary, cavity

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 2002/0032444 A1 (MISCHE) 14 March 2002 (14.03.2002), abstract, Fig. 1B, 2A, 10 and 12A, para [0004], [0018], [0023], [0029], [0034]-[0036].	1-22
Y	US 2007/0244485 A1 (GREENHALGH et al.) 18 October 2007 (18.10.2007), Fig. 1 an 72, para [0025], [0074], [0075], [0126], [0135], [0136], [0114].	1-22
Y	US 6,554,833 B2 (LEVY et al.) 29 April 2003 (29.04.2003), Fig. 6B	1-16

Further documents are listed in the continuation of Box C.


\* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E" earlier application or patent but published on or after the international filing date	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"O" document referring to an oral disclosure, use, exhibition or other means	"&" document member of the same patent family
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search  
27 February 2009 (27.02.2009)

Date of mailing of the international search report  
**10 MAR 2009**

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