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(71) Applicant(s)
MicroVention, Inc.

(72) Inventor(s)
Tieu, Tai D.;Martinez, George

(74) Agent / Attorney
Adams Pluck, SE 4 L 3 20 George St, Hornsby, NSW, 2077

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(71) Applicant (for all designated States except US): **MI-CROVENTION, INC.**; 75 Columbia, Suite A, Aliso Viejo, CA 92656 (US).

(72) Inventors; and

(75) Inventors/Applicants (for US only): **TIEU, Tai, D.** [US/US]; 15976 Mount Matterhorn Street, Fountain Valley, CA 92708 (US). **MARTINEZ, George** [US/US]; 528 Butte Court, Brea, CA 92821 (US).

(74) Agent: **SWANSON, Shane, S.**; Inskeep Intellectual Property Group, Inc., 2281 West 190th Street, Suite 200, Torrance, CA 90504 (US).

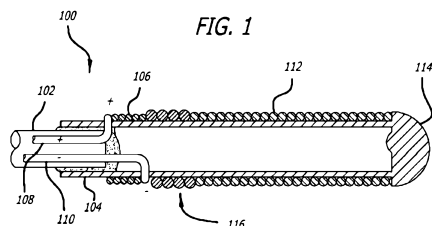
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(54) Title: A SYSTEM AND METHOD OF DETECTING IMPLANT DETACHMENT

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(57) Abstract: A system and method of detecting implant detachment within the body of a patient. The activation of the heater coil causes the degradation, melting or reduction of a component that brings the heater coil into or out of electrical contact with another component, or causes the individual loops of the coil to contact each other, thereby resulting in a notable change in resistance in the circuit supplying the heater coil with electricity.

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A SYSTEM AND METHOD OF DETECTING IMPLANT DETACHMENT

RELATED APPLICATIONS

[0001] The present application claims priority from U.S. Provisional Application Serial No. 61/016,180, filed December 21, 2007 entitled *A System and Method for Detecting Implant Detachment*, herein incorporated by reference in its entirety. This application also incorporates by reference U.S. Provisional Application Serial No. 60/604,671, filed August 25, 2004 entitled *Thermal Detachment System For Implantable Devices*; U.S. Provisional Application Serial No. 60/685,342 filed May 27, 2005 entitled *Thermal Detachment System For Implantable Devices*; U.S. Patent Application Serial No. 11/212,830 filed August 25, 2005 entitled *Thermal Detachment System For Implantable Devices*; U.S. Provisional Application Serial No. 60/952,520 filed July 27, 2007 entitled *Detachable Coil Incorporating Stretch Resistance*; and U.S. Provisional Application Serial No. 61/016,154 filed December 21, 2007 entitled *System and Method For Locating Detachment Zone Of A Detachable Implant*.

FIELD OF THE INVENTION

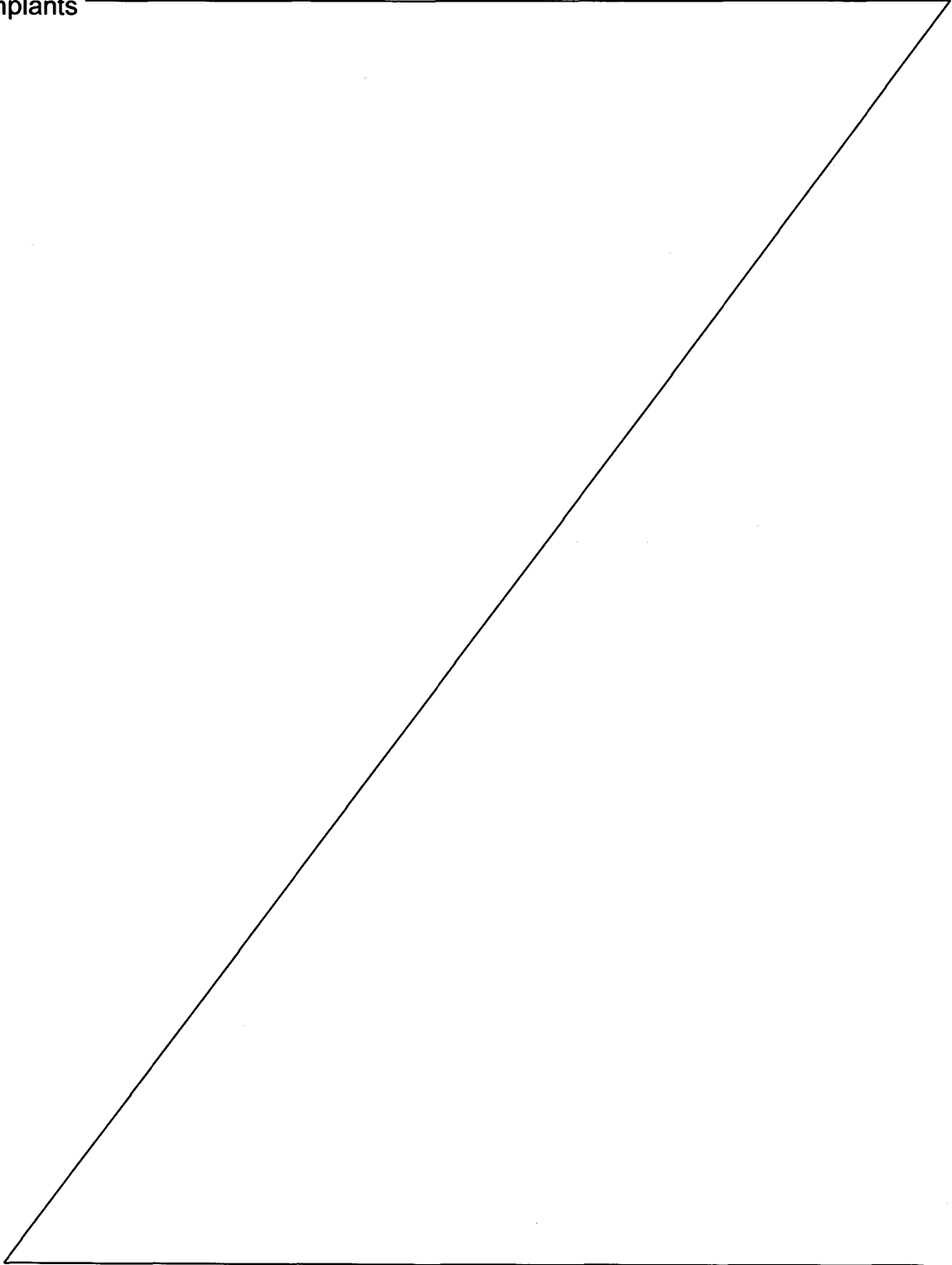
[0002] Embodiments of the present invention relate to systems and methods for delivering implant devices to a target site or location within the body of a patient. Embodiments of the present invention also relate to a method of detecting implant detachment within the body of a patient.

BACKGROUND OF THE INVENTION

[0002a] Any discussion of documents, acts, materials, devices, articles or the like which has been included in this specification is solely for the purpose of providing a context for the present invention. It is not to be taken as an admission that any or all of these matters form part of the prior art base or were common general knowledge in the field relevant to the present invention as it existed in Australia or elsewhere before the priority date of this application.

[0003] Delivery of implantable therapeutic devices by less invasive means has been demonstrated to be desirable in numerous clinical situations. For example, vascular embolization has been used to control vascular bleeding, to occlude the blood supply to tumors, to occlude fallopian tubes, and to occlude vascular aneurysms, particularly intracranial aneurysms. In recent years, vascular embolization for the treatment of aneurysms has received much attention.

Implants



used to treat aneurysms are often convoluted or coiled lengths of wound wire and are referred to as "microcoils." Microcoils work by filling an aneurysm causing the blood flow through the aneurysm to slow or stop, thereby inducing thrombosis within the aneurysm.

[0004] Microcoils are extremely flexible and have very little structural integrity. In order to make them easier to retrieve and reposition, recent efforts have been directed to making them stretch-resistant. For example, a stretch-resistant embolic coil having a stretch-resistant member passing through the interior lumen of the coil is described in U.S. Patent No. 5,582,619 to Ken, herein incorporated by reference in its entirety. U.S. Patent Publication No. 2004/0034363 to Wilson, herein incorporated by reference in its entirety, also discloses an embolic coil with a stretch resistant member having a distal end attached near the distal end of the coil and a proximal end of the member attached to a delivery catheter.

[0005] Several different treatment modalities have been employed in the prior art for deploying implant devices. For example, numerous repositionable detachment systems for implant devices have been described in the prior art including U.S. Patent No. 5,895,385 to Guglielmi et al. and 5,108,407 to Geremia et al., the contents of which are hereby incorporated by reference. Several systems, such as those disclosed in U.S. Patent No. 6,500,149 to Gandhi et al. and U.S. Patent No. 4,346,712 to Handa et al., the contents of which are hereby incorporated by reference, describe the use of a heater to detach and deploy the implant device.

[0006] While implant delivery and detachment systems are known in the art, they do not provide the user feedback that the implant has indeed detached from the delivery device. This is especially important in cases where the detachment relies on the application of heat or an electrolytic process where an element of time is involved. These delivery devices leave the user in the position of wondering whether heat etc., has been applied long enough to cause detachment. Hence, there exists a need for a method of detecting whether an implant has properly and effectively detached within the body of a patient.

SUMMARY OF THE INVENTION

[0006a] According to a first aspect of the present invention there is provided a system for detecting the detachment of an implant comprising: an implant advanced through a lumen by a pusher; a connector connecting said implant to said pusher; a heater located in proximity to said connector to release said implant and having a plurality of coils; said heater being in electrical communication with an indicator that communicates a change in state of the heater from an expanded state having a first gap size between at least some of said plurality of coils, to a contracted state having a second gap size between at least some of said plurality of coils; said second gap size being smaller than said first gap size; and, an expander contacting a portion of said heater and maintaining said heater in said expanded state until said heater causes said connector to release said implant.

[0006b] According to a second aspect of the present invention there is provided a method for detecting detachment of an implant at a vascular site, the method comprising the steps of: delivering an implant to a target site using a delivery device having a detachment mechanism; activating a heater coil within said delivery device; and, determining a change in gap size between at least some loops of said heater coil.

[0006c] According to another aspect of the present invention there is provided a method for detecting detachment of an implant, the method comprising the steps of: delivering an implant to a vascular site using a delivery device having a detachment mechanism; activating a heater coil within said delivery device; and monitoring for a change in gap size between at least some loops of said heater coil.

[0007] An embodiment of the present invention is an implant delivery and detachment system used to position and deploy implantable devices such as coils, stents, filters, and the like within a body cavity including, but not limited to, blood vessels, fallopian tubes, malformations such as fistula and aneurysms, heart defects (e.g. left atrial appendages and sepal openings), and other luminal organs.

[0008] An embodiment of the system comprises an implant, a delivery catheter (generically referred to as the pusher or delivery pusher), a detachable joint for

coupling the implant to the pusher, a heat generating apparatus (generically referred to as the heater), and a power source to apply energy to the heater.

[0009] An embodiment of the present invention also includes a method for detecting detachment of an implant. In particular, detachment of an implant may be detected by measuring the change in the electrical resistance of the delivery system.

[0010] An embodiment of the present invention may also be used in conjunction with the delivery mechanism disclosed in U.S. Patent Application No. 11/212,830 filed August 25, 2005 entitled "Thermal detachment system for implanting devices," which is incorporated by reference herein in its entirety.

[0011] In one embodiment of the present invention, the implant is coupled to the pusher using a tether, string, thread, wire, filament, fiber, or the like. Generically this is referred to as the tether. The tether may be in the form of a monofilament, rod, ribbon, hollow tube, or the like. Many materials can be used to detachably join the implant to the pusher. One class of materials are polymers such as polyolefin, polyolefin elastomer such as those made by Dow marketed under the trade name Engage or Exxon marketed under the trade name Affinity, polyethylene, polyester (PET), polyamide (Nylon), polyurethane, polypropylene, block copolymer such as PEBAX or Hytrel, and ethylene vinyl alcohol (EVA); or rubbery materials such as silicone, latex, and Kraton. In some cases, the polymer may also be cross-linked with radiation to manipulate its tensile strength and melt temperature. Another class of materials is metals such as nickel titanium alloy (Nitinol), gold, and steel. Preferably the selection of the material depends on the capacity of the material to store potential energy, the melting or softening temperature, the power used for detachment, and the body treatment site. The tether may be joined to the implant and/or the pusher by welding, knot tying, soldering, adhesive bonding, or other means known in the art. In one embodiment where the implant is a coil, the tether may run through the inside lumen of the coil and be attached to the distal end of the coil. This design not only joins the implant to the pusher, but also imparts stretch resistance to the coil without the use of a secondary stretch resistant member. In other embodiments where the implant is a coil, stent, or filter; the tether is attached to the proximal end of the implant.

[0012] In another embodiment of the present invention, the tether detachably coupling the implant to the pusher acts as a reservoir of stored (i.e. potential) energy that is released during detachment. This advantageously lowers the time and energy required to detach the implant because it allows the tether to be severed by application of heat without necessarily fully melting the material. The stored energy also may exert a force on the implant that pushes it away from the delivery catheter. This separation tends to make the system more reliable because it may prevent the tether from re-solidifying and holding the implant after detachment. Stored energy may be imparted in several ways. In one embodiment, a spring is disposed between the implant and pusher. The spring is compressed when the implant is attached to the pusher by joining one end of the tether to one of either the pusher or implant, pulling the free end of the tether until the spring is at least partially compressed, then affixing the free end of the tether to the other of the implant or the pusher. Since both ends of the tether are restrained, potential energy in the form of tension on the tether (or compression in the spring) is stored within the system. In another embodiment, one end of the tether is fixed as in the previous embodiment, and then the tether is placed in tension by pulling on the free end of the tether with a pre-determined force or displacement. When the free end of the tether is then affixed, the elongation (i.e. elastic deformation) of the tether material itself stores energy.

[0013] In another embodiment of the present invention, a heater is disposed on or within the pusher, typically, but not necessarily, near the distal end of the pusher. The heater may be attached to the pusher by, for example, soldering, welding, adhesive bonding, mechanical bonding, or other techniques known in the art. The heater may be in the form of a wound coil, heat pipe, hollow tube, band, hypotube, solid bar, toroid, or similar shape. The heater may be made from a variety of materials such as steel, chromium cobalt alloy, platinum, silver, gold, tantalum, tungsten, mangalin, chromium nickel alloy available from California Fine Wire Company under the trade name Stable Ohm, conductive polymer, or the like. The tether is disposed in proximity to the heater. The tether may pass through the lumen of a hollow or coil-type heater or may be wrapped around the heater. Although the tether may be disposed in direct contact with the heater, this is not necessary. For

ease of assembly, the tether may be disposed be in proximity to, but not actually touching, the heater.

[0014] Preferably the delivery catheter or pusher is an elongate member with distal and proximal ends adapted to allow the implant to be maneuvered to the treatment site. The pusher may comprise a core mandrel and one or more electrical leads to supply power to the heater. The pusher may taper in dimension and/or stiffness along the length, with the distal end usually being more flexible than the proximal end. In one embodiment, the pusher is adapted to be telescopically disposed within a delivery conduit such as a guide catheter or microcatheter. In another embodiment, the pusher contains an inner lumen allowing it to be maneuvered over a guide wire. In still another embodiment, the pusher can be maneuvered directly to the treatment site without a secondary device. The pusher may have a radiopaque marking system visible with fluoroscopy that allows it to be used in conjunction with radiopaque markings on the microcatheter or other adjunctive devices.

[0015] In another embodiment of the present invention, the core mandrel is in the form of a solid or hollow shaft, wire, tube, hypotube, coil, ribbon, or combination thereof. The core mandrel may be made from plastic materials such as PEEK, acrylic, polyamide, polyimide, Teflon, acrylic, polyester, block copolymer such as PEBAX, or the like. The plastic member(s) may be selectively stiffened along the length with reinforcing fibers or wires made from metal, glass, carbon fiber, braid, coils, or the like. Alternatively, or in combination with plastic components, metallic materials such as stainless steel, tungsten, chromium cobalt alloy, silver, copper, gold, platinum, titanium, nickel titanium alloy (Nitinol), and the like may be used to form the core mandrel. Alternatively, or in combination with plastic and/or metallic components, ceramic components such as glass, optical fiber, zirconium, or the like may be used to form the core mandrel. The core mandrel may also be a composite of materials. In one embodiment, the core mandrel comprises an inner core of radiopaque material such as platinum or tantalum and an outer covering of kink-resistant material such as steel or chromium cobalt. By selectively varying the thickness of the inner core, radiopaque identifiers can be provided on the pusher without using secondary markers. In another embodiment, a core material, for example stainless steel, with

desirable material properties such as kink resistance and/or compressive strength is selectively covered (by, for example, plating, drawing, or similar methods known in the art) with a low electrical resistance material such as copper, aluminum, gold, or silver to enhance its electrical conductivity, thus allowing the core mandrel to be used as an electrical conductor. In another embodiment, a core material, for example, glass or optical fiber, with desirable properties such as compatibility with Magnetic Resonance Imaging (MRI), is covered with a plastic material such as PEBAX or polyimide to prevent the glass from fracturing or kinking.

[0016] In another embodiment of the present invention, the heater is attached to the pusher, and then one or more electrical conductors are attached to the heater. In one embodiment a pair of conductive wires run substantially the length of the pusher and are coupled to the heater near the distal end of the pusher and to electrical connectors near the proximal end of the pusher. In another embodiment, one conductive wire runs the substantially the length of the pusher and the core mandrel itself is made from a conductive material or coated with a conductive material to act as a second electrical lead. Preferably the wire and the mandrel are coupled to the heater near the distal end and to one or more connectors near the proximal end of the pusher. In another embodiment, a bipolar conductor is coupled to the heater and is used in conjunction with radiofrequency (RF) energy to power the heater. In any of the embodiments, the conductor(s) may run in parallel to the core mandrel or may pass through the inner lumen of a substantially hollow core mandrel (for example, a hypotube).

[0017] In another embodiment of the present invention, an electrical and/or thermally insulating cover or sleeve may be placed over the heater. The sleeve may be made from insulating materials such as polyester (PET), Teflon, block copolymer, silicone, polyimide, polyamide, and the like.

[0018] In another embodiment of the present invention, electrical connector(s) are disposed near the proximal end of the pusher so that the heater can be electrically connected to a power source through the conductors. In one embodiment, the connectors are in the form of a plug with one or more male or female pins. In another embodiment, the connector(s) are tubes, pins, or foil that can be connected with clip-

type connectors. In another embodiment, the connector(s) are tubes, pins, or foil that are adapted to mate with an external power supply.

[0019] In another embodiment of the present invention, the pusher connects to an external power source so that the heater is electrically coupled to the power source. Preferably the power source may be from battery(s) or connected to the electrical grid by a wall outlet. The power source supplies current in the form of direct current (DC), alternating current (AC), modulated direct current, or radiofrequency (RF) at either high or low frequency. The power source may be a control box that operates outside of the sterile field or may be a hand-held device adapted to operate within a sterile field. The power source may be disposable, rechargeable, or may be reusable with disposable or rechargeable battery(s).

[0020] In another embodiment of the present invention, the power source may comprise an electronic circuit that assists the user with detachment. In one embodiment, the circuit detects detachment of the implant and provides a signal to the user when detachment has occurred. In another embodiment, the circuit comprises a timer that provides a signal to the user when a pre-set length of time has elapsed. In another embodiment, the circuit monitors the number of detachments and provides a signal or performs an operation such as locking the system off when a pre-set number of detachments have been performed. In another embodiment, the circuit comprises a feedback loop that monitors the number of attachment attempts and increases the current, voltage, and/or detachment time in order to increase the likelihood of a successful detachment.

[0021] In another embodiment of the present invention, the construction of the system allows for extremely short detachment time. In one embodiment the detachment time is less than 1 second.

[0022] In another embodiment of the present invention, the construction of the system minimizes the surface temperature of the device during detachment. In one embodiment, the surface temperature at the heater during detachment is under 50°C. In another embodiment, the surface temperature at the heater during detachment is under 42°C.

[0023] In another embodiment of the present invention, detachment of the implant is detected by measuring a change in the electrical resistance of the delivery system, specifically the heater zone, to detect implant detachment.

[0023a] Throughout this specification, the word "comprise", or variations thereof such as "comprises" or "comprising", will be understood to imply the inclusion of a stated element, integer or step, or group of elements integers or steps, but not the exclusion of any other element, integer or step, or group of elements, integers or steps.

[0024] These and other aspects and features of the present invention will be appreciated upon consideration of the following drawings and detailed descriptions, which are provided by way of example only.

BRIEF DESCRIPTION OF THE DRAWINGS

[0025] Figure 1 illustrates a cross-sectional side view of a first embodiment of a detachment system according to the present invention;

[0026] Figure 2 illustrates a cross-sectional side view of a second embodiment of a detachment system according to the present invention;

[0027] Figure 3A illustrates example direct signaling current according to the present invention;

[0028] Figure 3B illustrates example alternating signaling current according to the present invention;

[0029] Figure 4 illustrates a cross-sectional side view of a third embodiment of a detachment system according to the present invention;

[0030] Figure 5 illustrates example temperature data of the surface of a detachment system as a function of time according to the present invention;

[0031] Figure 6 illustrates a cross-sectional side view of an electrical connector of a detachment system according to the present invention;

[0032] Figure 7 illustrates a cross-sectional side view of radiopaque layers of a detachment system according to the present invention; and

[0033] Figure 8 illustrates a cross-sectional side view of a detachment system including a stent according to the present invention;

[0034] Figure 9 illustrates a side view of a implant device according to the present invention;

[0035] Figure 10 illustrates a perspective view of a coil and expander of the delivery system of Figure 9;

[0036] Figure 11 illustrates a partial cut-away view of a coil and expander in an expanded state over a pusher of a delivery system according to the present invention; and

[0037] Figure 12 illustrates a partial cut-away view of a system according to Figure 11 in a contracted state.

DETAILED DESCRIPTION OF THE INVENTION

[0038] Turning to Figure 1, a detachment system 100 of the present invention, and specifically the distal portion of the detachment system 100, is illustrated. The detachment system 100 includes a pusher 102 that is preferably flexible. The pusher 102 is configured for use in advancing an implant device 112 into and within the body of a patient and, specifically, into a target cavity site for implantation and delivery of the implant device 112. Potential target cavity sites include but are not limited to blood vessels and vascular sites (e.g., aneurysms and fistula), heart openings and defects (e.g., the left atrial appendage), and other luminal organs (e.g., fallopian tubes).

[0039] A stretch-resistant tether 104 detachably couples the implant 112 to the pusher 102. In this example, the tether 104 is a plastic tube that is bonded to the pusher 102. A substantially solid cylinder could also be a design choice for the tether 104. The stretch resistant tether 104 extends at least partially through the interior lumen of an implant device 112.

[0040] Near the distal end of the pusher 102, a heater 106 is disposed in proximity to the stretch resistant tether 104. The heater 106 may be wrapped around the stretch resistant tether 104 such that the heater 106 is exposed to or otherwise in direct contact with the blood or the environment, or alternatively may be insulated by a sleeve, jacket, epoxy, adhesive, or the like. The pusher 102 comprises a pair of electrical wires, positive electrical wire 108 and negative electrical wire 110. The wires 108 and 110 are coupled to the heater 106 by any suitable means, such as, e.g., by welding or soldering.

[0041] The electrical wires 108, 110 are capable of being coupled to a source of electrical power (not shown). As illustrated the negative electrical wire 110 is coupled to the distal end of the heater 106 and the positive electrical wire 108 is coupled to the proximal end of the heater 106. In another embodiment, this configuration may be reversed, i.e., the negative electrical wire 110 is coupled to the proximal end of the heater 106 while the positive electrical wire 108 is coupled to the distal end of the heater 106.

[0042] Energy is applied to the heater 106 from the electrical wires 108, 110 in order to sever the portion of the tether 104 in the proximity of the heater 106. It is not necessary for the heater 106 to be in direct contact with the tether 104. The heater 106 merely should be in sufficient proximity to the tether 104 so that heat generated by the heater 106 causes the tether 104 to sever. As a result of activating the heater 106, the section of the stretch resistant tether 104 that is approximately distal from the heater 106 and within the lumen of an implant device 112 is released from the pusher 102 along with the implant device 112.

[0043] As illustrated, the implant device 112 is an embolic coil. An embolic coil suitable for use as the implant device 112 may comprise a suitable length of wire

formed into a helical microcoil. The coil may be formed from a biocompatible material including platinum, rhodium, palladium, rhenium, tungsten, gold, silver, tantalum, and various alloys of these metals, as well as various surgical grade stainless steels. Specific materials include the platinum/tungsten alloy known as Platinum 479 (92% Pt, 8% W, available from Sigmund Cohn, of Mount Vernon, N.Y.) and nickel/titanium alloys (such as the nickel/titanium alloy known as Nitinol).

[0044] Another material that may be advantageous for forming the coil is a bimetallic wire comprising a highly elastic metal with a highly radiopaque metal. Such a bimetallic wire would also be resistant to permanent deformation. An example of such a bimetallic wire is a product comprising a Nitinol outer layer and an inner core of pure reference grade platinum, available from Sigmund Cohn, of Mount Vernon, N.Y., and Anomet Products, of Shrewsbury, Mass.

[0045] Commonly-assigned U.S. Patent No. 6,605,101 provides a further description of embolic coils suitable for use as the implant device 112, including coils with primary and secondary configurations wherein the secondary configuration minimizes the degree of undesired compaction of the coil after deployment. The disclosure of U.S. Patent No. 6,605,101 is fully incorporated herein by reference. Furthermore, the implant device 112 may optionally be coated or covered with a hydrogel or a bioactive coating known in the art.

[0046] The coil-type implant device 112 resists unwinding because the stretch resistant tether 104 that extends through the lumen of the implant device 112 requires substantially more force to plastically deform than the implant device 112 itself. The stretch resistant tether 104 therefore assists in preventing the implant device 112 from unwinding in situations in which the implant device 112 would otherwise unwind.

[0047] During assembly, potential energy may be stored within the device to facilitate detachment. In one embodiment, an optional spring 116 is placed between the heater 106 and the implant device 112. The spring is compressed during assembly and the distal end of the tether 104 may be tied or coupled to the distal end of the implant device 112, or may be melted or otherwise formed into an atraumatic distal end 114.

[0048] In one embodiment, the stretch resistant tether 104 is made from a material such as a polyolefin elastomer, polyethylene, or polypropylene. One end of the tether 104 is attached to the pusher 102 and the free end of the tether 104 is pulled through the implant 112 with the proximal end of the implant 112 flush to either the heater 106 (if no spring 116 is present) or to the compressed spring 116. A pre-set force or displacement is used to pre-tension the tether 104, thus storing energy in an axial orientation (i.e. co-linear or parallel to the long axis of the pusher 102) within the tether 104. The force or displacement depends on the tether material properties, the length of the tether 104 (which itself depends on the tether's attachment point on the pusher and the length of the implant). Generally, the force is below the elastic limit of the tether material, but sufficient to cause the tether to sever quickly when heat is applied. In one preferred embodiment wherein the implant to be deployed is a cerebral coil, the tether has a diameter within the range of approximately .001 to .007 inches. Of course the size of the tether can be changed to accommodate different types and sizes of other implants as necessary.

[0049] Turning to Figure 2, another embodiment of a detachment system of the present invention, detachment system 200, is illustrated. Detachment system 200 shares several common elements with detachment system 100. For example, the same devices usable as the implant device 112 with detachment system 100 are also usable as the implant device 112 with detachment system 200. These include, e.g., various embolic microcoils and coils. The implant device 112 has been previously described with respect to detachment system 100. As with the implant device 112, the same identification numbers are used to identify other elements/components of detachment system 100 that may correspond to elements/components of detachment system 200. Reference is made to the description of these elements in the description of detachment system 100 as that description also applies to these common elements in detachment system 200.

[0050] With detachment system 200, an interior heating element 206 is used to separate a section of a stretch resistant tube 104 and an associated implant device 112 from the detachment system 200. Detachment system 200 includes a delivery pusher 202 that incorporates a core mandrel 218. The detachment system 200

further includes a positive electrical wire 208 and a negative electrical wire 210 that extend through the lumen of the delivery pusher 202.

[0051] To form the internal heating element 206, the positive electrical wire 208 and the negative electrical wire 210 may be coupled to the core mandrel 218 of the delivery pusher 202. Preferably, the electrical wires 208, 210 are coupled to a distal portion of the core mandrel 218.

[0052] In one embodiment, the positive electrical wire 208 is coupled to a first distal location on the core wire 218, and the negative electrical wire 210 is coupled to a second distal location on the core wire 218, with the second distal location being proximal to the first distal location. In another embodiment, the configuration is reversed, i.e., the positive electrical wire 208 is coupled to the second distal location and the negative electrical wire 210 is coupled to the first distal location on the core wire 218. When the positive electrical wire 208 and the negative electrical wire 210 are coupled to the distal portion of the core mandrel 218, the distal portion of the core mandrel 218 along with the electrical wires 208, 210 forms a circuit that is the interior heating element 206.

[0053] The heater 206 increases in temperature when a current is applied from a power source (not shown) that is coupled to the positive electrical wire 208 and the negative electrical wire 210. If a greater increase in temperature/higher degree of heat is required or desired, a relatively high resistance material such as platinum or tungsten may be coupled to the distal end of the core mandrel 218 to increase the resistance of the core mandrel 218. As a result, higher temperature increases are produced when a current is applied to the heater 206 than would be produced with a lower resistance material. The additional relatively high resistance material coupled to the distal end of the core mandrel 218 may take any suitable form, such as, e.g., a solid wire, a coil, or any other shape or material as described above.

[0054] Because the heater 206 is located within the lumen of the tube-shaped tether 104, the heater 206 is insulated from the body of the patient. As a result, the possibility of inadvertent damage to the surrounding body tissue due to the heating of the heater 206 may be reduced.

[0055] When a current is applied to the heater 206 formed by the core mandrel 218, the positive electrical wire 208, and the negative electrical wire 210, the heater 206 increases in temperature. As a result, the portion of the stretch resistant tether 104 in proximity to the heater 206 severs and is detached, along with the implant device 112 that is coupled to the tether 104, from the detachment system 200.

[0056] In one embodiment of the detachment system 200, the proximal end of the stretch resistant tether 104 (or the distal end of a larger tube (not shown) coupled to the proximal end of the stretch resistant tether 104) may be flared in order to address size constraints and facilitate the assembly of the detachment system 200.

[0057] In a similar manner as with detachment system 100, energy may be stored within the system with, for example, an optional compressive spring 116 or by pre-tensioning the tether 104 during assembly as previously described. When present, the release of potential energy stored in the system operates to apply additional pressure to separate the implant device 112, and the portion of the stretch resistant tether 104 to which the implant device 112 is coupled, away from the heater 206 when the implant device 112 is deployed. This advantageously lowers the required detachment time and temperature by causing the tether 104 to sever and break.

[0058] As with detachment system 100, the distal end of the stretch resistant tether 104 of detachment system 200 may be tied or coupled to the distal end of the implant device 112, or may be melted or otherwise formed into an atraumatic distal end 114.

[0059] Figure 4 illustrates another preferred embodiment of a detachment system 300. In many respects, the detachment system 300 is similar to the detachment system 200 shown in Figure 2 and detachment system 100 shown in Figure 1. For example, the detachment system 300 includes a delivery pusher 301 containing a heater 306 that detaches an implant device 302. Detachment system 300 also utilizes a tether 310 to couple the implant device 302 to the delivery pusher 301.

[0060] In the cross-sectional view of Figure 4, a distal end of the delivery pusher 301 is seen to have a coil-shaped heater 306 that is electrically coupled to electrical wires 308 and 309. These wires 308, 309 are disposed within the delivery pusher 301, exiting at a proximal end of the delivery pusher 301 and coupling to a power supply (not shown). The tether 310 is disposed in proximity to the heater 306, having a proximal end fixed within the delivery pusher 301 and a distal end coupled to the implant device 302. As current is applied through wires 308 and 309, the heater 306 increases in temperature until the tether 310 breaks, releasing the implant device 302.

[0061] To reduce the transfer of heat from the heater 306 to the surrounding tissue of the patient and to provide electrical insulation, an insulating cover 304 is included around at least the distal end of the outer surface of the delivery pusher 301. As the thickness of the cover 304 increases, the thermal insulating properties also increase. However, increased thickness also brings increased stiffness and a greater diameter to the delivery pusher 301 that could increase the difficulty of performing a delivery procedure. Thus, the cover 304 is designed with a thickness that provides sufficient thermal insulating properties without overly increasing its stiffness.

[0062] To enhance attachment of the tether 310 to the implant device 302, the implant device 302 may include a collar member 322 welded to the implant device 302 at weld 318 and sized to fit within the outer reinforced circumference 312 of the delivery pusher 301. The tether 310 ties around the proximal end of the implant device 302 to form knot 316. Further reinforcement is provided by an adhesive 314 that is disposed around the knot 316 to prevent untying or otherwise unwanted decoupling.

[0063] In a similar manner as with detachment systems 100 and 200, energy may be stored within the system with, for example, an optional compressive spring (similar to compressive spring 116 in Figure 1 but not shown in Figure 4) or by axially pre-tensioning the tether 104 during assembly. In this embodiment, one end of the tether 310 is attached near the proximal end of the implant device 302 as previously described. The free end of the tether 310 is threaded through a distal portion of the

delivery pusher 301 until it reaches an exit point (not shown) of the delivery pusher 301. Tension is applied to the tether 310 in order to store energy in the form of elastic deformation within the tether material by, for example, placing a pre-determined force on the free end of the tether 310 or moving the taut tether 310 a pre-determined displacement. The free end of the tether 310 is then joined to the delivery pusher 301 by, for example, tying a knot, applying adhesive or similar methods known in the art.

[0064] When present, the release of potential energy stored in the system operates to apply additional pressure to separate the implant device 302, and the portion of the tether 310 to which the implant device 302 is coupled, away from the heater 306 when the implant device 302 is deployed. This advantageously lowers the required detachment time and temperature by causing the tether 310 to sever and break.

[0065] The present invention also provides for methods of using detachment systems such as detachment systems 100, 200, or 300. The following example relates to the use of detachment system 100, 200, or 300 for occluding cerebral aneurysms. It will, however, be appreciated that modifying the dimensions of the detachment system 100, 200, or 300 and the component parts thereof and/or modifying the implant device 112, 302 configuration will allow the detachment system 100, 200, or 300 to be used to treat a variety of other malformations within a body.

[0066] With this particular example, the delivery pusher 102, 202, or 301 of the detachment system 100, 200, or 300 may be approximately 0.010 inches to 0.030 inches in diameter. The tether 104, 310 that is coupled near the distal end of the delivery pusher 102, 202, or 301 and is coupled to the implant device 112, 302 may be 0.0002 inches to 0.020 inches in diameter. The implant device 112, 302; which may be a coil, may be approximately 0.005 inches to 0.020 inches in diameter and may be wound from 0.0005 inch to 0.005 inch wire.

[0067] If potential energy is stored within the detachment system 100, 200, or 300, the force used to separate the implant 112, 302 from the pusher typically ranges up to 250 grams force.

[0068] The delivery pusher 102, 202, or 301 may comprise a core mandrel 218 and at least one electrically conductive wire 108, 110, 208, 210, 308, or 309. The core mandrel 218 may be used as an electrical conductor, or a pair of conductive wires may be used, or a bipolar wire may be used as previously described.

[0069] Although the detachment systems 100, 200, and 300 have been illustrated as delivering a coil, other implant devices are contemplated in the present invention. For example, Figure 8 illustrates the detachment system 300 as previously described in Figure 4 having an implant that is a stent 390. This stent 390 could similarly be detached by a similar method as previously described in regards to the detachment systems 100, 200, and 300. In a further example, the detachment systems 100, 200, or 300 may be used to deliver a filter, mesh, scaffolding or other medical implant suitable for delivery within a patient.

[0070] Figure 7 presents an embodiment of a delivery pusher 350, which could be used in any of the embodiments as delivery pusher 102, 202, or 301, which includes radiopaque materials to communicate the position of the delivery pusher 350 to the user. Specifically, the radiopaque marker material is integrated into the delivery pusher 350 and varied in thickness at a desired location, facilitating easier and more precise manufacturing of the final delivery pusher 350.

[0071] Prior delivery pusher designs, such as those seen in U.S. Patent 5,895,385 to Guglielmi, rely on high-density material such as gold, tantalum, tungsten, or platinum in the form of an annular band or coil. The radiopaque marker is then bonded to other, less dense materials, such as stainless steel, to differentiate the radiopaque section. Since the radiopaque marker is a separate element placed at a specified distance (often about 3 cm) from the tip of the delivery pusher, the placement must be exact or the distal tip of the delivery pusher 350 can result in damage to the aneurysm or other complications. For example, the delivery pusher 350 may be overextended from the microcatheter to puncture an aneurysm. Additionally, the manufacturing process to make a prior delivery pusher can be difficult and expensive, especially when bonding dissimilar materials.

[0072] The radiopaque system of the present invention overcomes these disadvantages by integrating a first radiopaque material into most of the delivery pusher 350 while varying the thickness of a second radiopaque material, thus eliminating the need to bond multiple sections together. As seen in Figure 7, the delivery pusher 350 comprises a core mandrel 354 (i.e. the first radiopaque material), preferably made from radiopaque material such as tungsten, tantalum, platinum, or gold (as opposed to the mostly radiolucent materials of the prior art designs such as steel, Nitinol, and Elgiloy).

[0073] The delivery pusher 350 also includes a second, outer layer 352, having a different radiopaque level. Preferably, outer layer 352 is composed of a material having a lower radiopaque value than the core mandrel 354, such as Elgiloy, Nitinol, or stainless steel (commercially available from Fort Wayne Metals under the trade name DFT). In this respect, both the core mandrel 354 and the outer layer 352 are visible and distinguishable from each other under fluoroscopy. The outer layer 352 varies in thickness along the length of the delivery pusher 350 to provide increased flexibility and differentiation in radio-density. Thus the thicker regions of the outer layer 352 are more apparent to the user than the thinner regions under fluoroscopy.

[0074] The transitions in thickness of the outer layer 352 can be precisely created at desired locations with automated processes such as grinding, drawing, or forging. Such automated processes eliminate the need for hand measuring and placement of markers and further eliminates the need to bond a separate marker element to other radiolucent sections, thus reducing the manufacturing cost and complexity of the system.

[0075] In the present embodiment, the delivery pusher 350 includes three main indicator regions of the outer layer 352. A proximal region 356 is the longest of the three at 137 cm, while a middle region 358 is 10 cm and a distal region 360 is 3 cm. The length of each region can be determined based on the use of the delivery pusher 350. For example, the 3 cm distal region 360 may be used during a coil implant procedure, as known in the art, allowing the user to align the proximal edge of the distal region 360 with a radiopaque marker on the microcatheter within which the

delivery pusher 350 is positioned. The diameter of each of the regions depends on the application and size of the implant. For a typical cerebral aneurysm application for example, the proximal region 356 may typically measure .005-.015 inches, the middle region 358 may typically measure .001-.008 inches, while the distal region 360 may typically measure .0005-.010 inches. The core mandrel 354 will typically comprise between about 10-80% of the total diameter of the delivery pusher 350 at any point.

[0076] Alternately, the delivery pusher 350 may include any number of different regions greater than or less than the three shown in Figure 7. Additionally, the radiopaque material of the core mandrel 354 may only extend partially through the delivery pusher 350. For example, the radiopaque material could extend from the proximal end of the core mandrel 354 to three centimeters from the distal end of the delivery pusher 350, providing yet another predetermined position marker visible under fluoroscopy.

[0077] In this respect, the regions 356, 358, and 360 of delivery pusher 350 provide a more precise radiopaque marking system that is easily manufactured, yet is readily apparent under fluoroscopy. Further, the increased precision of the markers may decrease complications relating to improper positioning of the delivery pusher during a procedure.

[0078] In operation, the microcatheter is positioned within a patient so that a distal end of the microcatheter is near a target area or lumen. The delivery pusher 350 is inserted into the proximal end of the microcatheter and the core mandrel 354 and outer layer 352 are viewed under fluoroscopy. The user aligns a radiopaque marker on the microcatheter with the beginning of the distal region 360, which communicates the location of the implant 112, 302 relative to the tip of the microcatheter.

[0079] In some situations, for example, small aneurysms where there may be an elevated risk of vessel damage from the stiffness of the delivery pusher 350, the user may position the proximal end of the implant slightly within the distal end of the microcatheter during detachment. The user then may push the proximal end of the implant 112, 302 out of the microcatheter with the next coil, an adjunctive device such

as guidewire, or the delivery pusher 102, 202, 301, or 350. In another embodiment, the user may use the radiopaque marking system to locate the distal end of the delivery pusher outside the distal end of the microcatheter.

[0080] Once the implant device 112, 302 of the detachment system 100, 200, or 300 is placed in or around the target site, the operator may repeatedly reposition the implant device 112, 302 as necessary or desired.

[0081] When detachment of the implant device 112, 302 at the target site is desired, the operator applies energy to the heater 106, 206, or 306 by way of the electrical wires 108, 110, 208, 210, 308, or 309. The electrical power source for the energy may be any suitable source, such as, e.g., a wall outlet, a capacitor, a battery, and the like. For one aspect of this method, electricity with a potential of approximately 1 volt to 100 volts is used to generate a current of 1 milliamp to 5000 milliamps, depending on the resistance of the detachment system 100, 200, or 300.

[0082] One embodiment of a connector system 400 that can be used to electrically couple the detachment system 100, 200, or 300 to the power source is shown in Figure 6. The connector system 400 includes an electrically conductive core mandrel 412 having a proximal end surrounded by an insulating layer 404. Preferably the insulating layer 404 is an insulating sleeve such as a plastic shrink tube of polyolefin, PET, Nylon, PEEK, Teflon, or polyimide. The insulating layer 404 may also be a coating such as polyurethane, silicone, Teflon, paralyene. An electrically conductive band 406 is disposed on top of the insulating layer 404 and secured in place by molding bands 414, adhesive, or epoxy. Thus, the core mandrel 412 and the conductive band 406 are electrically insulated from each other. The conductive band 406 is preferably composed of any electrically conductive material, such as silver, gold, platinum, steel, copper, conductive polymer, conductive adhesive or similar materials, and can be a band, coil, or foil. Gold is especially preferred as the conductive material of the conductive band 406 because of the ability of gold to be drawn into a thin wall and its ready availability. The core mandrel 412 has been previously described and may be plated with, for example, gold, silver, copper, or aluminum to enhance its electrical conductivity.

[0083] The connector system 400 also includes two electrical wires 408 and 410 which connect to the conductive band 406 and core member 412, respectively, and to a heating element at the distal end of a delivery system such as those described in Figures 1, 2, and 4 (not shown in Figure 6). These wires 408 and 410 are preferably connected by soldering, brazing, welding, laser bonding, or conductive adhesive, or similar techniques.

[0084] Once the user is ready to release the implant 112, 302 within the patient, a first electrical clip or connector from a power source is connected to a non-insulated section 402 of the core mandrel 412 and a second electrical clip or connector from the power source is connected to the conductive band 406. Electrical power is applied to the first and second electrical clips, forming an electrical circuit within the detachment system 100, 200, or 300, causing the heater 106, 206, or 306 to increase in temperature and sever the tether 104, 310.

[0085] Once the detachment system 100, 200, or 300 is connected to the power source the user may apply a voltage or current as previously described. This causes the heater 106, 206, or 306 to increase in temperature. When heated, the pre-tensioned tether 104, 310 will tend to recover to its unstressed (shorter) length due to heat-induced creep. In this respect, when the tether 104, 310 is heated by the heater 106, 206, or 306; its overall size shrinks. However, since each end of the tether 104, 310 is fixed in place as previously described, the tether 104, 310 is unable to shorten in length, ultimately breaking to release the implant device 112, 302.

[0086] Because there is tension already within the system in the form of a spring 116 or deformation of the tether material 104, 310; the amount of shrinkage required to break the tether 104, 310 is less than that of a system without a pre-tensioned tether. Thus, the temperature and time required to free the implant device 112, 302 is lower.

[0087] Figure 5 is a graph showing the temperatures at the surface of the PET cover 304 of the detachment system 300. As can be seen, the surface temperature of the detachment system 300 during detachment does not vary linearly with time. Specifically, it only takes just under 1 second for the heat generated by the heating

coil 306 to penetrate the insulating cover 304. After 1 second, the surface temperature of the insulating cover 304 dramatically increases. Although different outer insulating material may slightly increase or decrease this 1-second surface temperature window, the necessarily small diameter of the detachment system 100, 200, or 300 prevents providing a thick insulating layer that may more significantly delay a surface temperature increase.

[0088] It should be understood that the embodiments of the detachment system 100, 200, or 300 include a variety of possible constructions. For example, the insulating cover 304 may be composed of Teflon, PET, polyamide, polyimide, silicone, polyurethane, PEEK, or materials with similar characteristics. In the embodiments 100, 200, or 300 the typical thickness of the insulating cover is .0001-.040 inches. This thickness will tend to increase when the device is adapted for use in, for example, proximal malformations, and decrease when the device is adapted for use in more distal, tortuous locations such as, for example, cerebral aneurysms.

[0089] In order to minimize the damage and possible complications caused by such a surface temperature increase, the present invention detaches the implant device 112, 302 before the surface temperature begins to significantly increase. Preferably, the implant device 112, 302 is detached in less than a second, and more preferably, in less than 0.75 seconds. This prevents the surface temperature from exceeding 50°C (122° F), and more preferably, from exceeding 42°C (107°F).

[0090] Once the user attempts to detach the implant device 112, 302, it is often necessary to confirm that the detachment has been successful. The circuitry integrated into the power source may be used to determine whether or not the detachment has been successful. In one embodiment of the present invention an initial signaling current is provided prior to applying a detachment current (i.e. current to activate the heater 106, 206, or 306 to detach an implant 112, 302). The signaling current is used to determine the inductance in the system before the user attempts to detach the implant and therefore has a lower value than the detachment current, so as not to cause premature detachment. After an attempted detachment, a similar signaling current is used to determine a second inductance value that is compared to

the initial inductance value. A substantial difference between the initial inductance and the second inductance value indicates that the implant 112, 302 has successfully been detached, while the absence of such a difference indicates unsuccessful detachment. In this respect, the user can easily determine if the implant 112, 302 has been detached, even for delivery systems that utilize nonconductive temperature sensitive polymers to attach an implant, such as those seen in Figures 1, 2, and 4.

[0091] In the following description and examples, the terms “current” and “electrical current” are used in the most general sense and are understood to encompass alternating current (AC), direct current (DC), and radiofrequency current (RF) unless otherwise noted. The term “changing” is defined as any change in current with a frequency above zero, including both high frequency and low frequency. When a value is measured, calculated and/or saved, it is understood that this may be done either manually or by any known electronic method including, but not limited to, an electronic circuit, semiconductor, EPROM, computer chip, computer memory such as RAM, ROM, or flash; and the like. Finally, wire windings and toroid shapes carry a broad meaning and include a variety of geometries such as circular, elliptical, spherical, quadrilateral, triangular, and trapezoidal shapes.

[0092] When a changing current passes through such objects as wire windings or a toroid, it sets up a magnetic field. As the current increases or decreases, the magnetic field strength increase or decreases in the same way. This fluctuation of the magnetic field causes an effect known as inductance, which tends to oppose any further change in current. Inductance (L) in a coil wound around a core is dependant on the number of turns (N), the cross-sectional area of the core (A), the magnetic permeability of the core (μ), and length of the coil (l) according to equation 1 below:

Equation 1.

$$L = \frac{0.4\pi N^2 A \mu}{l}$$

[0093] The heater 106 or 306 is formed from a wound coil with proximal and distal electrically conductive wires 108, 110, 308, or 309 attached to a power source. The tether 104, 310 has a magnetic permeability μ_1 and is positioned through the center of the resistive heater, having a length l, cross sectional area A, and N winds,

forming a core as described in the previous equation. Prior to detachment, a changing signaling current i_1 , such as the waveforms shown in Figures 3A and 3B, with frequency f_1 , is sent through the coil windings. This signaling current is generally insufficient to detach the implant. Based on the signaling current, the inductive resistance X_L (i.e. the electrical resistance due to the inductance within the system) is measured by an electronic circuit such as an ohmmeter. The initial inductance of the system L_1 is then calculated according to the formula:

Equation 2.

$$L_1 = \frac{X_L}{2\pi f_1}$$

[0094] This initial value of the inductance L_1 depends on the magnetic permeability μ_1 of the core of the tether 104, 310 according to Equation 1, and is saved for reference. When detachment is desired, a higher current and/or a current with a different frequency than the signaling current is applied through the resistive heater coil, causing the tether 104, 310 to release the implant 112, 302 as previously described. If detachment is successful, the tether 104, 310 will no longer be present within the heater 106, 306 and the inside of the heater 106, 306 will fill with another material such as the patient's blood, contrast media, saline solution, or air. This material now within the heater core will have a magnetic permeability μ_2 that is different than the tether core magnetic permeability μ_1 .

[0095] A second signaling current and frequency f_2 is sent through the heater 106, 306 and is preferably the same as the first signaling current and frequency, although one or both may be different without affecting the operation of the system. Based on the second signaling current, a second inductance L_2 is calculated. If the detachment was successful, the second inductance L_2 will be different (higher or lower) than the first inductance L_1 due to the difference in the core magnetic permeabilities μ_1 and μ_2 . If the detachment was unsuccessful, the inductance values should remain relatively similar (with some tolerance for measurement error). Once detachment has been confirmed by comparing the difference between the two inductances, an alarm or signal can be activated to communicate successful

detachment to the user. For example, the alarm might include a beep or an indicator light.

[0096] Preferably, the delivery system 100, 300 used according to this invention connects to a device that automatically measures inductance at desired times, performs required calculations, and signals to the user when the implant device has detached from the delivery catheter. However, it should be understood that part or all of these steps can be manually performed to achieve the same result.

[0097] The inductance between the attached and detached states can also preferably be determined without directly calculating the inductance. For example, the inductive resistance XL can be measured and compared before and after detachment. In another example, the detachment can be determined by measuring and comparing the time constant of the system, which is the time required for the current to reach a predetermined percentage of its nominal value. Since the time constant depends on the inductance, a change in the time constant would similarly indicate a change in inductance.

[0098] The present invention may also include a feedback algorithm that is used in conjunction with the detachment detection described above. For example, the algorithm automatically increases the detachment voltage or current automatically after the prior attempt fails to detach the implant device. This cycle of measurement, attempted detachment, measurement, and increased detachment voltage/current continues until detachment is detected or a predetermined current or voltage limit is attained. In this respect, a low power detachment could be first attempted, followed automatically by increased power or time until detachment has occurred. Thus, battery life for a mechanism providing the detachment power is increased while the average coil detachment time is greatly reduced.

[0099] Referring now to Figures 9 through 12, there is shown an embodiment of a delivery system 500 for use with the present invention that includes a detachment detection capability. The delivery system 500 operates under the principle that electrical current passing through a coil held in an expanded, open gap configuration will encounter more resistance than electrical current passing through a coil in a

contracted, closed gap configuration. In the expanded configuration, the electrical current must follow the entire length of the coiled wire. In the contracted configuration, the electrical current can bridge the coils and travel in a longitudinal direction.

[00100] The delivery system 500, illustrated in Figure 9, is generally similar to the previously described detachment system 300 of the present invention seen in Figure 4, including a delivery pusher 301, containing a heater coil 306 that detaches an implant device 302. The detachment system 500 similarly utilizes a tether 310 to couple the implant device 302 to the delivery pusher 301.

[00101] The heater coil 306 is preferably a resistance-type heater having a plurality of loops 306A, as seen in Figure 10, that connect to a voltage source through a connector system at the proximal end of the delivery pusher 301, such as the connector system 400 described in Figure 6.

[00102] The delivery system 500 also includes a heater coil expander 502 that serves two functions. First, it expands the heater coil 306 such that the heater coil 306 maintains a friction-fit attachment to the inside of the insulating cover 309, thereby connecting the two. Second, the heater coil expander 502 expands the heater coil 306 in such a manner that electricity is forced to flow around each individual loop 306A of the coil 306 in order to maximize the resistance of the coil 306.

[00103] Maximizing the coil resistance not only serves to heat the coil 306 when voltage is passed through it, it also sets an initial value (or "normal" value) for the resistance provided by the coil 306, which can be used to compare a changed resistance state, indicating detachment of the implant 302. Hence, the heater coil expander 502 must also be capable of undergoing change when subjected to heat. In this regard, the heater coil expander 502 may be made of any suitable sturdy material capable of holding the heater coil 306 in an expanded, biased state while also being capable of melting or being otherwise reduced by the heat of the heater coil 306 in order to yield to the bias of the heater coil 306 to return to an unbiased state. Examples of acceptable materials include, but are not limited to, polymers and monofilament.

[00104] It will be appreciated that the energy necessary to break the tether 310 will be predetermined and will constitute a lower energy than the predetermined energy necessary to transform or to otherwise melt or reduce the heater expander 502. Accordingly, it will be possible determine that the tether 310 will have been broken and the implant 302 detached when the resistance of the heater coil 306 changes due to the transformation of the heater expander 502.

[00105] The heater coil expander 502 shown in Figures 9 and 10 operates by longitudinally, or radially and longitudinally, expanding a heater coil 306 which is normally a closed gap coil in a relaxed state. In other words, the individual loops 306A contact each other when the heater coil 306 is not stretched or radially expanded. Preferably, the heater coil expander 502 may have a coiled shape as seen in Figure 10. Alternately, the heater coil expander may have a continuous, tubular shape with helical ridges. It should be understood that a variety of different expander shapes that expand the loops 306A of the heater coil 306 from each other are suitable for use in the present invention.

[00106] Preferably the power source (previously described in this embodiment and connected to the connector system 400) also includes a measuring instrument for measuring the resistance of the heater coil 306. In this respect, the power source (preferably located in a hand-sized unit) includes an indicator that communicates when a change in resistance has occurred and therefore when detachment of the implant has occurred.

[00107] An alternative embodiment of the heater coil expander 512 is shown in Figures 11 and 12. The heater coil expander 512 operates in conjunction with the heater coil 306 so that the heater loops are in an open gap state, as shown in Figure 11, and a pusher 350, as previously described with reference to Figure 7, that conducts electricity. The heater coil 306 is sized to snugly fit around the pusher 350 in a contracted state. The heater coil expander 512 operates to separate the heater coil 306 from the pusher 350, electrically isolating the heater coil 306 therefrom, as illustrated in Figure 11. As the heat from the heater coil 306 melts or otherwise reduces or degrades the heater coil expander 512, the heater coil 306 resumes a

contracted state (i.e., reduced diameter configuration), making electrical, if not physical, contact with the pusher 350, as shown in Figure 12. In this respect the individual loops are shortened, significantly reducing the resistance of the circuit and thereby indicating detachment has occurred.

[00108] Another alternative embodiment of the present invention, the heater coil expander 502 may be sized to expand the heater coil 306 against a conductive reinforcement circumference 312, shown in Figure 9. Hence, when the heater coil 306 is in its initial expanded position and in contact with the electrically conductive reinforcement circumference 312, the loops 306A of heater coil 306 are shorted and maintain a low initial resistance that is registered by the controller for the circuit (i.e., the measurement device of the power source).

[00109] When the heater coil 306 is energized, the initial resistance is noted and the heater coil expander 502 melts, degrades or otherwise reduces. The heater coil 306 then contracts, releasing the conductive reinforcement circumference 312, and the implant 302. The loop 306A of heater coil 306 are no longer shorted out by the reinforcement circumference 312, and the circuit experiences a change in resistance as the electrical current must travel through each of the individual loops 306A. This increase in resistance signifies the implant 302 is detached.

[00110] Although the invention has been described in terms of particular embodiments and applications, one of ordinary skill in the art, in light of this teaching, can generate additional embodiments and modifications without departing from the spirit of or exceeding the scope of the claimed invention. For example, the heater coil or heater coil expander could be constructed to activate a switch that provides a user indication of detachment in some manner. Additionally, a visual indicator may be associated with the change in resistance to provide easy indication of detachment. Accordingly, it is to be understood that the drawings and descriptions herein are proffered by way of example to facilitate comprehension of the invention and should not be construed to limit the scope thereof.

What is claimed is:

1. A system for detecting the detachment of an implant comprising:
an implant advanced through a lumen by a pusher;
a connector connecting said implant to said pusher;
a heater located in proximity to said connector to release said implant and having a plurality of coils; said heater being in electrical communication with an indicator that communicates a change in state of the heater from an expanded state having a first gap size between at least some of said plurality of coils, to a contracted state having a second gap size between at least some of said plurality of coils; said second gap size being smaller than said first gap size; and,
an expander contacting a portion of said heater and maintaining said heater in said expanded state until said heater causes said connector to release said implant.
2. The system of claim 1 wherein a dimension of the heater is greater in the expanded state relative to the dimension in a contracted state.
3. The system of claim 1 or 2 wherein the heater has a resistance that is higher in the expanded state relative to the resistance in a contracted state.
4. The system of any one of the preceding claims wherein the pusher is conductive.
5. The system of claim 4 wherein the heater physically contacts the pusher when the heater is in a contracted state.
6. The system of any one of the preceding claims wherein the heater is a resistance-type heater.
7. The system of any one of the preceding claims wherein adjacent portions of the heater are maintained apart from one another in the expanded state.
8. The system of claim 1 wherein the heater has a resistance that is higher in a contracted state relative to the resistance in the expanded state.

9. The system of any one of the preceding claims wherein the heater contacts an interior surface of a conductive collar in the expanded state.
10. The system of any one of the preceding claims wherein the expander changes physical form when the expander is heated.
11. The system of any one of the preceding claims wherein a volume of the expander decreases when the expander is heated.
12. The system of any one of the preceding claims wherein the expander is a polymer.
13. A method for detecting detachment of an implant at a vascular site, the method comprising the steps of:
 - delivering an implant to a target site using a delivery device having a detachment mechanism;
 - activating a heater coil within said delivery device; and,
 - determining a change in gap size between at least some loops of said heater coil.
14. The method of claim 13 wherein said determining a change in gap size further comprises determining a decrease in said gap size between at least some loops of said heater coil.
15. The method of claim 13 wherein determining a change in gap size further comprises monitoring for a decreased electrical resistance of said heater coil.
16. The method of claim 13 wherein said determining a change in gap size further comprises determining contact between at least some of said loops of said heater.
17. The method of any one of claims 13 to 16 further comprising displacing an expander separating at least some of said loops of said heater.

18. The method of any one of claims 13 to 17 further comprising changing a physical form of an expander separating at least some of said loops of said heater.

19. A method for detecting detachment of an implant, the method comprising the steps of:

delivering an implant to a vascular site using a delivery device having a detachment mechanism;

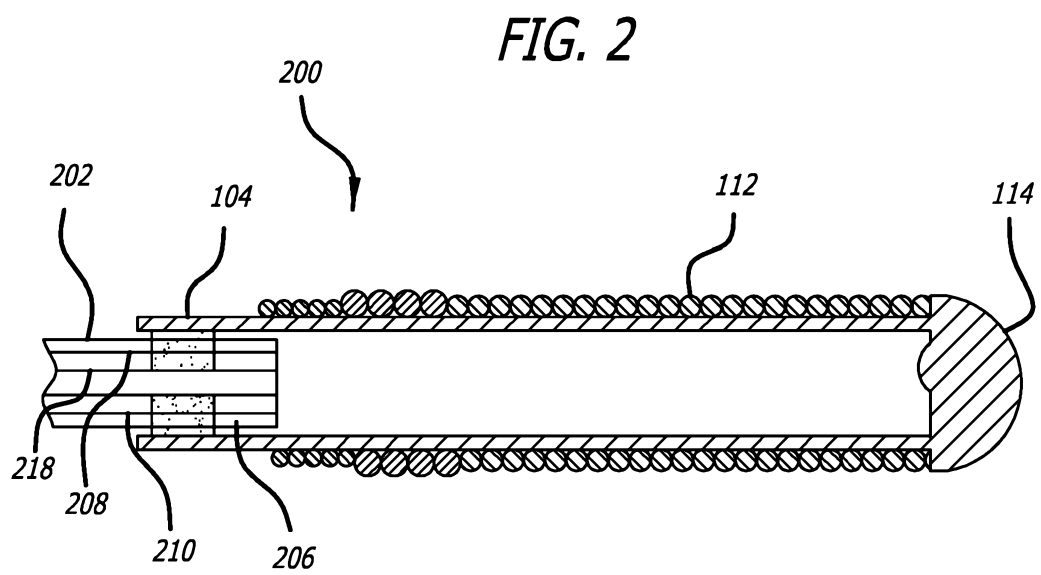
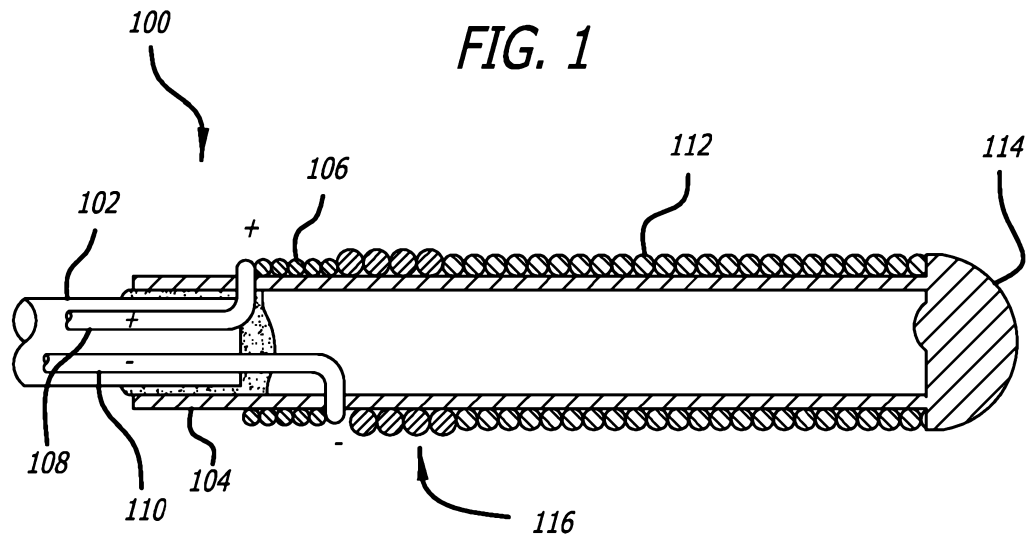
activating a heater coil within said delivery device; and

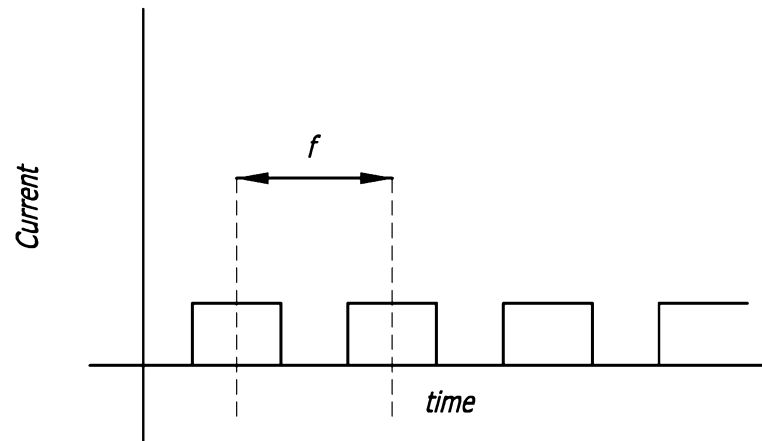
monitoring for a change in gap size between at least some loops of said heater coil.

20. The method of claim 19, further comprising melting an expander member that maintains said loops in a spaced-apart configuration.

21. A system substantially as hereinbefore described with reference to any one or more of the examples and/or the accompanying drawings.

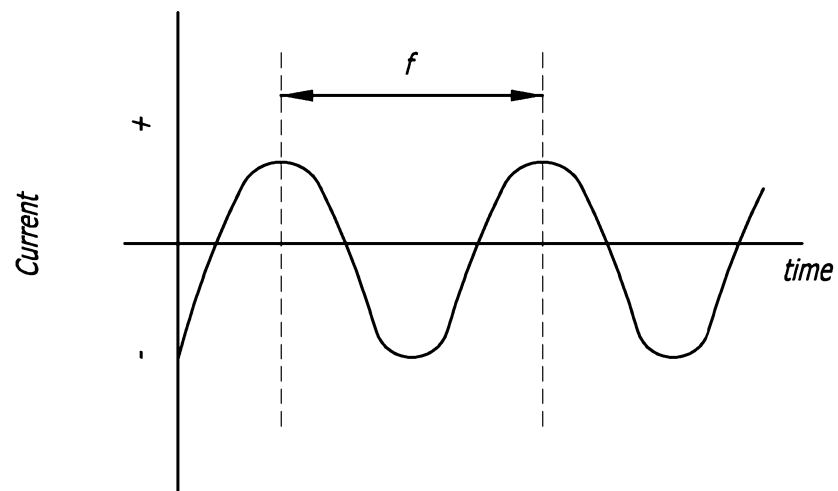
22. A method substantially as hereinbefore described with reference to any one or more of the examples and/or the accompanying drawings.





*Direct Current (DC)
Signaling*

FIG. 3A



*Alternating Current (AC)
Signaling*

FIG. 3B

FIG. 4

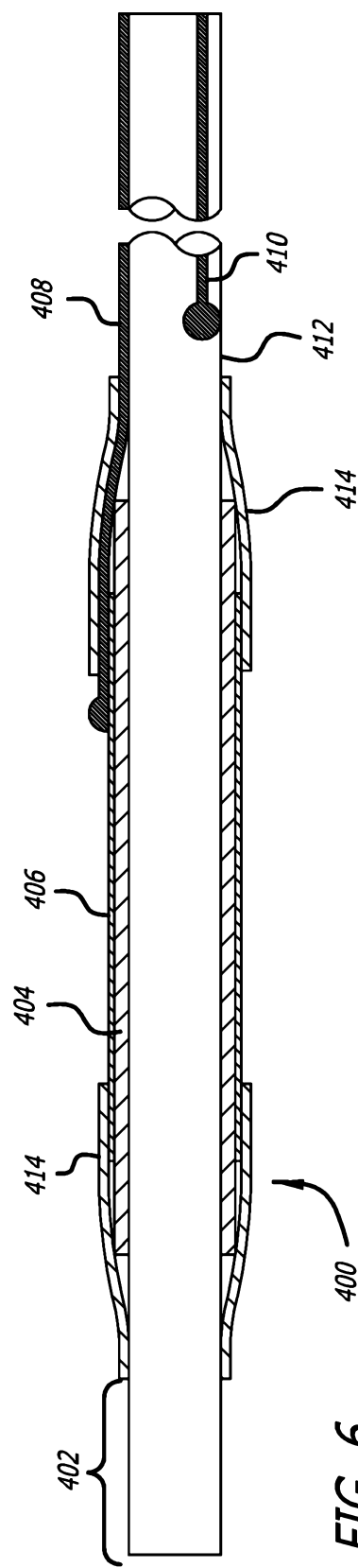
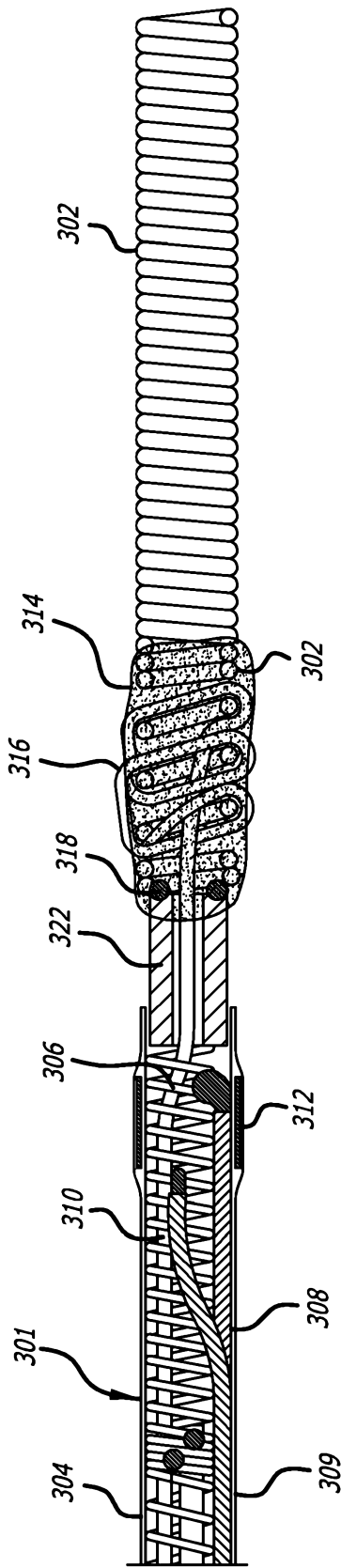
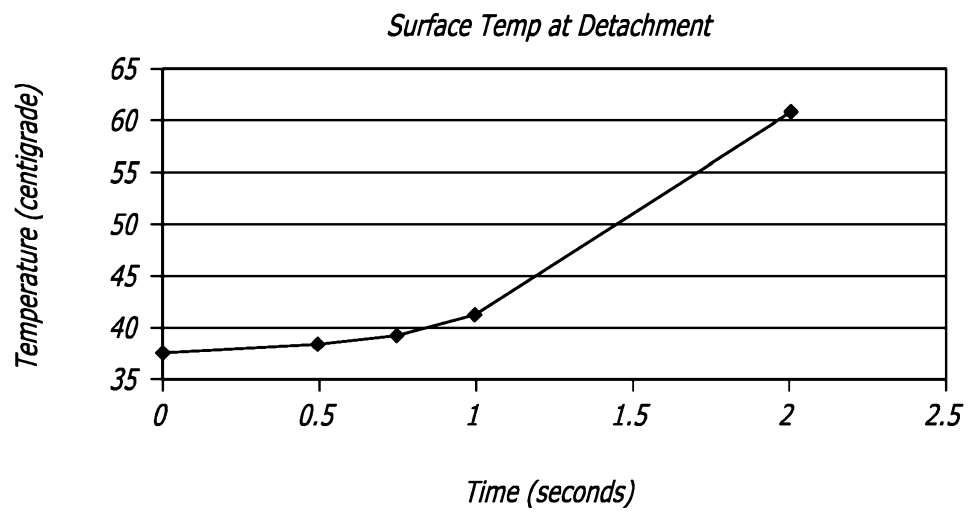
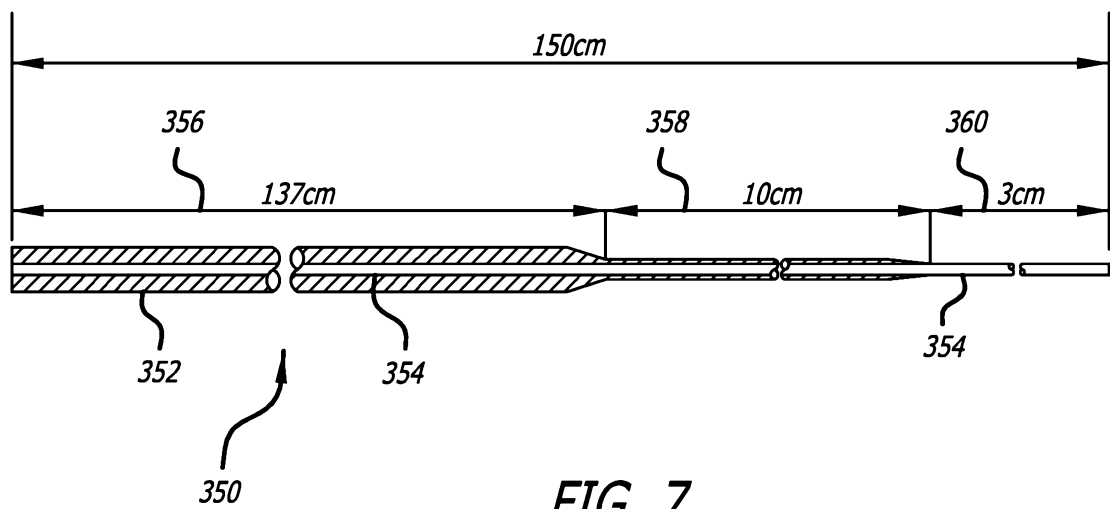


FIG. 6

**FIG. 5****FIG. 7**

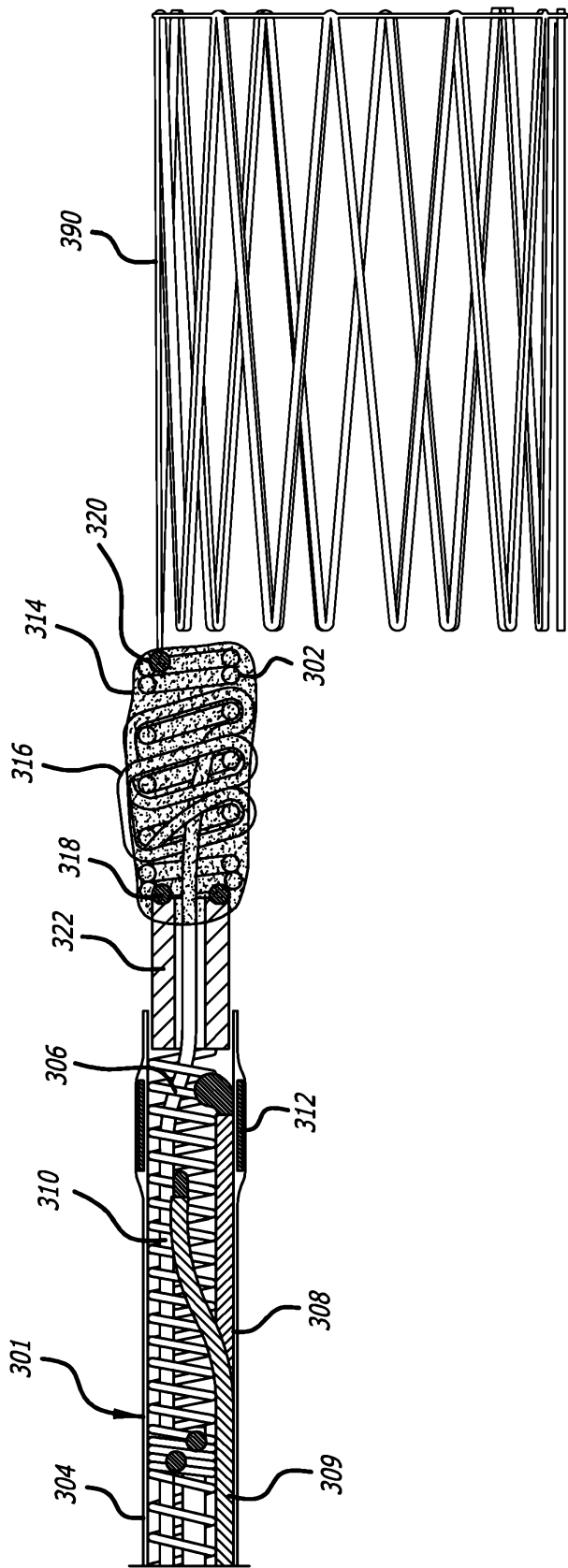
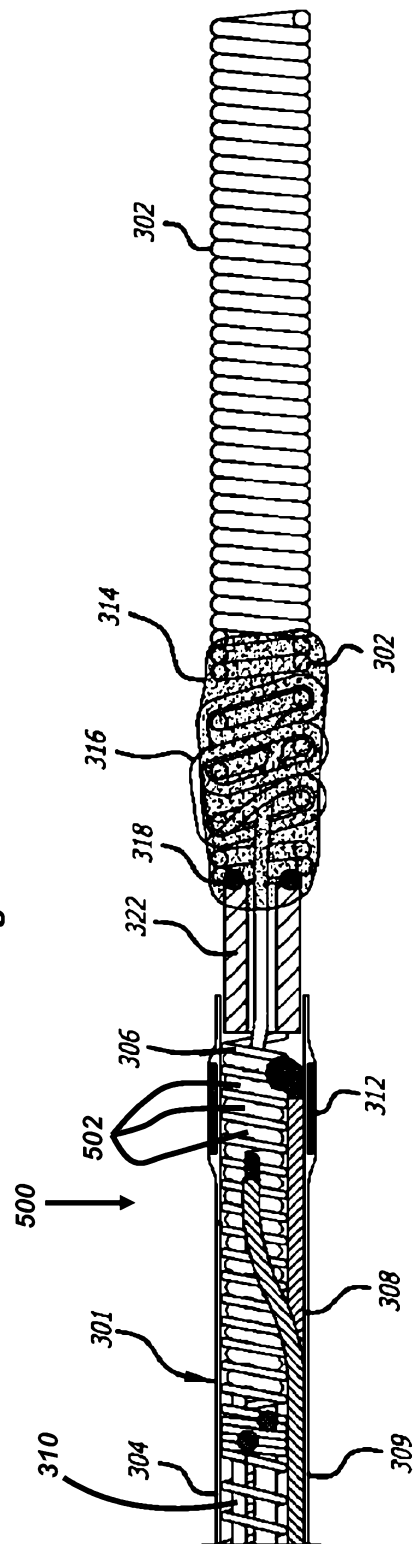
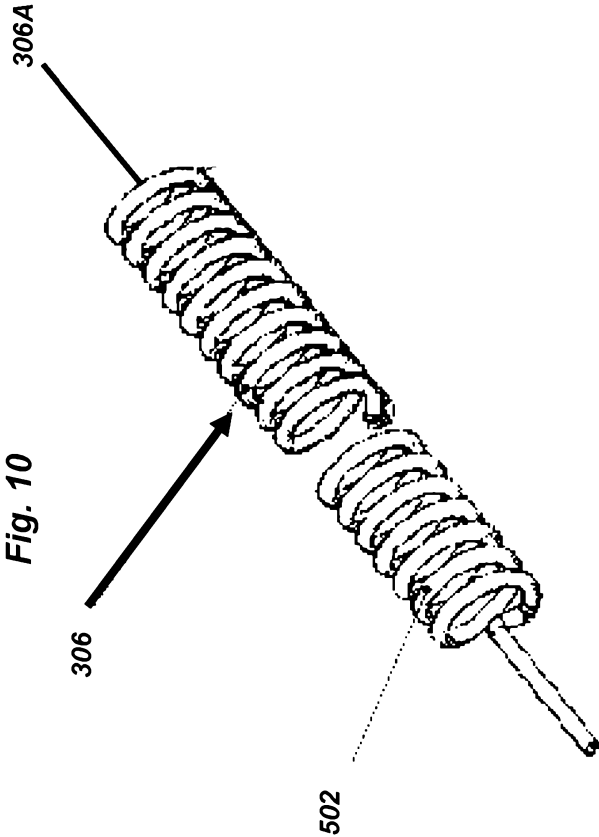


FIG. 8

Fig. 9





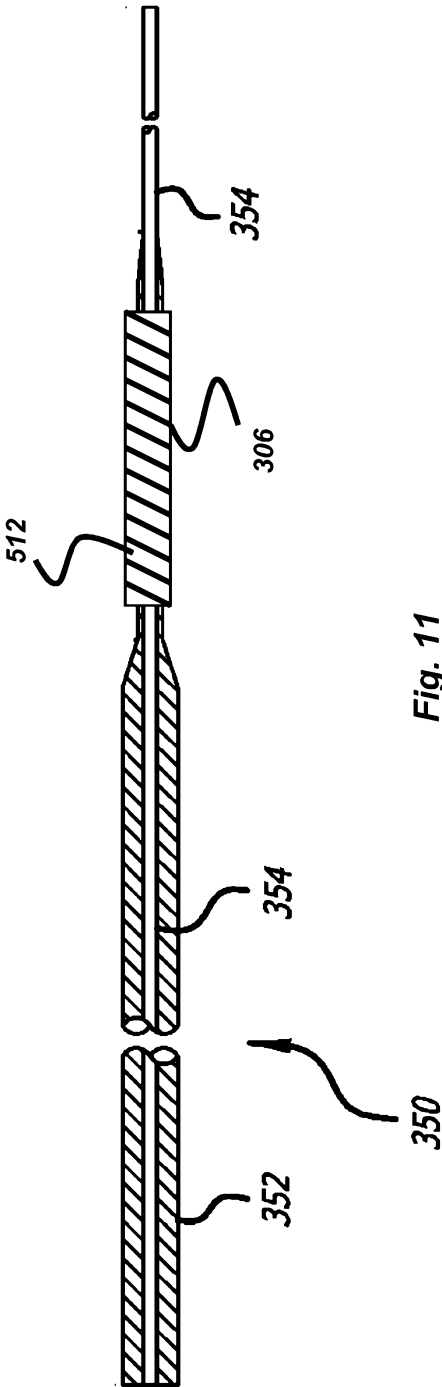


Fig. 11

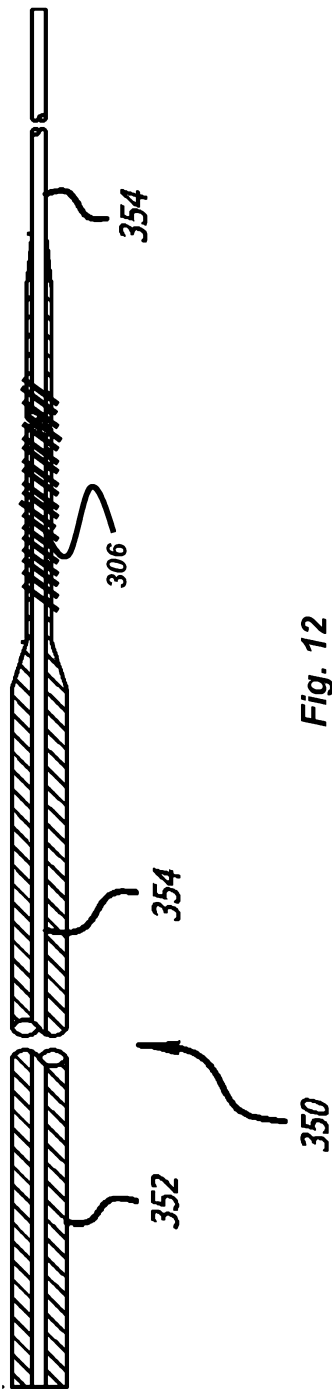


Fig. 12