



(86) Date de dépôt PCT/PCT Filing Date: 2009/12/24
(87) Date publication PCT/PCT Publication Date: 2010/07/01
(45) Date de délivrance/Issue Date: 2013/12/17
(85) Entrée phase nationale/National Entry: 2011/06/27
(86) N° demande PCT/PCT Application No.: KR 2009/007804
(87) N° publication PCT/PCT Publication No.: 2010/074540
(30) Priorités/Priorities: 2008/12/26 (KR10-2008-0134459);
2009/12/24 (KR10-2009-0130794)

(51) Cl.Int./Int.Cl. *A61K 9/127* (2006.01),
A61K 31/353 (2006.01), *A61K 31/56* (2006.01),
A61K 31/70 (2006.01), *A61K 31/7105* (2006.01),
A61K 31/711 (2006.01), *A61K 39/21* (2006.01),
A61K 39/235 (2006.01)

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(54) Titre : COMPOSITION PHARMACEUTIQUE CONTENANT UN MEDICAMENT ANIONIQUE ET PROCEDE DE
PREPARATION ASSOCIE
(54) Title: PHARMACEUTICAL COMPOSITION CONTAINING AN ANIONIC DRUG, AND A PRODUCTION METHOD
THEREFOR

(57) **Abrégé/Abstract:**

Disclosed are an anionic drug-containing pharmaceutical composition comprising: an anionic drug as an active ingredient; a cationic lipid; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, and a method for preparing the same. The pharmaceutical composition may increase stability of the anionic drug in blood or in a body fluid, and it may enable intracellular delivery to improve efficacy of anionic drugs.



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ABSTRACT

Disclosed are an anionic drug-containing pharmaceutical composition comprising: an anionic drug as an active ingredient; a cationic lipid; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, and a method for preparing the same. The pharmaceutical composition may increase stability of the anionic drug in blood or in a body fluid, and it may enable intracellular delivery to improve efficacy of anionic drugs.

PHARMACEUTICAL COMPOSITION CONTAINING AN ANIONIC DRUG, AND A PRODUCTION METHOD THEREFOR

□Technical Field of the Invention□

This disclosure relates to an anionic drug-containing pharmaceutical composition comprising: an anionic drug as an active ingredient; a cationic lipid; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, and a method of preparing the same.

□Background of the Invention□

Safe and efficient drug delivery technologies have been studied for a long time in the treatment using anionic drugs, particularly nucleic acid material, and various delivery systems and delivery technologies have been developed. Particularly, delivery technologies using a viral delivery system using adenovirus or retrovirus, etc., and a non-viral delivery system using cationic lipids, cationic polymers, etc. have been developed.

However, a technology using a viral delivery system is exposed to a risk such as non-specific immune reaction, etc., and it is known to have a lot of problems in commercialization due to the complex production process. Therefore, recent studies are progressed toward a non-viral delivery system using cationic lipids or cationic polymers to improve the disadvantages. Although the non-viral delivery system has inferior efficiency to the viral delivery system, it has less side effects and the production cost is inexpensive compared with viral delivery system.

Many studies have been conducted on non-viral delivery system used for delivery of nucleic acid material, and most representative examples thereof include a complex of cationic lipid and nucleic acid (lipoplex) and a complex of a polycationic polymer and nucleic acid (polyplex). Many studies on the cationic lipid or polycationic polymer have been progressed because it stabilizes anionic drugs by forming a complex by electrostatic interactions with the anionic drug and facilitates intracellular delivery (De Paula D, Bentley MV, Mahato RI, Hydrophobization and bioconjugation for enhanced siRNA delivery and targeting, RNA 13

(2007) 431-56; Gary DJ, Puri N, Won YY, Polymer-based siRNA delivery: Perspectives on the fundamental and phenomenological distinctions from polymer-based DNA delivery, J Control release 121 (2007) 64-73).

However, if cationic lipids or polycationic polymers studied so far are used in an amount required to obtain sufficient effects, serious toxicity, although less than viral delivery system, may be caused and thus it may be improper for the therapeutic use. And, although a lipid-nucleic acid complex which forms a complex compound through a bond between a cationic lipid and nucleic acid is widely used in a cell line experiment, it does not form a structure that can be stable in blood, and thus it cannot be used in the living body (see US 6,458,382).

A nucleic acid-cationic liposome complex or a cationic liposome comprising nucleic acid, which is one of the non-viral delivery system commonly used to deliver nucleic acid into the cells in the living body, consists of an amphiphilic lipid, a neutral lipid and a fusogenic lipid, etc., and nucleic acid material is attached to the outside of the liposome by electrostatic bond or captured inside (US2003-0073640, WO05/007196, US2006-0240093). However, the liposome delivery system may be easily captured by reticuloendothelial system (RES) and exhibit side effects with significant toxicity, and thus, it may not be appropriate for systemic application. And, another non-viral delivery system commonly used includes a cationic polymer, and a polycationic polymer including multivalent cationic charge per a polymer is predominantly used therefore. Particularly, commonly used polymer is polycationic polyethyleneimine (PEI), and the polycationic polymer binds with nucleic acid material by electrostatic interaction to form a nucleic acid-polymer complex thereby forming a nanoparticle. However, the polycationic polymer such as polyethyleneimine promotes apoptosis, and it is known that cytotoxicity increases as the molecular weight and the degree of branching of the polymer increase. Although polycationic polymers with low molecular weight are known to have low cytotoxicity, they cannot form an effective complex due to low charge density of the polymer, and thus, they cannot show the sufficient intracellular delivery and the sufficient stability in blood.

Therefore, it is required to develop an anionic drug delivery technology using the minimal amount of cationic polymer or cationic lipid to decrease toxicity, which is stable in blood and body fluid, and enables intracellular delivery to obtain sufficient effects. The delivery

system using the nucleic acid material directly conjugated with a lipid or a polymer is being studied, but if a lipid or a polymer is directly conjugated with nucleic acid material, there are difficulties in terms of conjugation efficiency or quality control.

Meanwhile, there have been various attempts to use amphiphilic block copolymer as a drug delivery system that can solubilize a poorly water-soluble drug by forming a polymeric micelle and stabilize a poorly water-soluble drug in an aqueous solution (Korean Registered Patent No. 0180334). However, since the amphiphilic block copolymer cannot enclose hydrophilic drug such as nucleic acid in the polymeric micelle, it is not suitable for delivery of anionic drug including nucleic acid.

Meanwhile, many diseases result from the overexpression of disease genes or the expression of mutated genes. Since siRNA (short interfering RNA) inhibits the expression of specific genes in a sequence specific manner, it is highlighted as a therapeutic nucleotide drug. Particularly, siRNA is expected to overcome the problems of the antisense nucleotide or ribozyme because siRNA has more potency and more accurate gene selectivity compared with the antisense nucleotide or ribozyme. The siRNA is a short double-stranded RNA molecule and the number of nucleotides in each strand ranges from 15 to 30, and it inhibits the expression of corresponding gene by cleaving mRNA of gene with a sequence complementary thereto (McManus and Sharp, *Nature Rev. Genet.* 3:737 (2002); Elbashir, et al., *Genes Dev.* 15:188 (2001).

However, despite these advantages, siRNA is known to be rapidly degraded by nuclease in blood and rapidly excreted from the body through a kidney. It is also known that siRNA cannot easily pass a cell membrane because it is strongly negatively charged. Therefore, to use siRNA as a therapeutic agent, it is required to develop a delivery system that may stabilize siRNA in blood, may efficiently deliver it into target cells, and does not show toxicity.

□Detailed Description of the Invention□

□Technical Problem□

Accordingly, one aspect of the present invention provides a pharmaceutical composition capable of effectively delivering anionic drugs in the body.

Another aspect of the present invention provides a method of preparing the

pharmaceutical composition capable of effectively delivering anionic drugs in the body.

□Technical Solution□

The pharmaceutical composition according to the present invention comprises
 an anionic drug as an active ingredient;
 a cationic lipid; and
 an amphiphilic block copolymer,

wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer. According to one embodiment of the present invention, the pharmaceutical composition may further comprise a fusogenic lipid. The composition may be used for delivery of the anionic drug contained as the active ingredient.

Another embodiment provides use of a composition comprising an anionic drug as an active ingredient; a cationic lipid; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, for delivery of an anionic drug.

Yet another embodiment provides a method of delivering an anionic drug comprising the administration of a composition comprising: an anionic drug as an active ingredient; a cationic lipid; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, to a patient in need thereof. The patient may include mammals, preferably human, primates, rodents, and the like.

And, a method of preparing the composition according to the present invention may comprise:

- (a) dissolving the anionic drug and the cationic lipid in a water-miscible organic solvent or a mixed solvent of an aqueous solution and an organic solvent so as to separate the phases;
- (b) separating the organic solvent layer of (a);
- (c) mixing the organic solvent of (b) with the amphiphilic block copolymer and removing the organic solvent; and
- (d) adding an aqueous solution to the mixture from which the organic solvent is

removed so as to form a micelle

According to another embodiment, a method of preparing the composition according to the present invention may comprise:

(a) dissolving the anionic drug, the cationic lipid and the amphiphilic block copolymer in a water-miscible organic solvent or a mixed solvent of an aqueous solution and an organic solvent;

(b) removing the organic solvent layer of (a); and

(c) adding an aqueous solution to the mixture of (b) from which the organic solvent is removed so as to form a micelle.

Hereinafter, the present invention will be explained in detail.

According to one embodiment, the anionic drug and the cationic lipid are entrapped in the micelle structure of the amphiphilic block copolymer while forming a complex of the anionic drug and the lipid by electrostatic interactions.

Fig. 1 schematically shows the structure of the polymeric micelle delivery system according to one embodiment of the present invention in which the anionic drug and the cationic lipid are enclosed. As shown in Fig. 1, the anionic drug binds to the cationic lipid by electrostatic interactions, so as to form a complex of the anionic drug and the cationic lipid, and the formed complex of the anionic drug and the cationic lipid is entrapped in the micelle structure of the amphiphilic block copolymer.

When the complex of the anionic drug and the cationic lipid is entrapped in the micelle structure of the amphiphilic block copolymer, it may have improved stability in blood or in a body fluid. According to one embodiment, the particle size of the micelle may be 10 to 200 nm, specifically 10 to 150 nm. The particle size is determined considering the stability of the micelle structure, the contents of the constitutional ingredients, absorption of anionic drugs in the body, and convenience of sterilization as a pharmaceutical composition.

The anionic drug may include any material that is negatively charged in an aqueous solution and has pharmacological activity. According to one embodiment, the anionic property may be provided from at least one functional group selected from the group consisting of carboxylic group, phosphate group, and sulfate group. According to one embodiment, the anionic drug may be a multi-anionic drug or nucleic acid.

The nucleic acid may be a nucleic acid drug such as polynucleotide derivatives wherein deoxyribonucleic acid, ribonucleic acid or backbone, sugar or base is chemically modified or the end is modified, and more specific examples may include RNA, DNA, siRNA (short interfering RNA), aptamer, antisense ODN (oligodeoxynucleotide), antisense RNA, ribozyme, DNzyme, and a combination thereof. And, the backbone, sugar or base of the nucleic acid may be modified or the end may be modified for the purpose of increasing blood stability or weakening immune reactions, and the like. Specifically, a part of phosphodiester bond of nucleic acid may be substituted by phosphorothioate or boranophosphate bond, or at least one kind of nucleotide wherein various functional groups such as methyl group, methoxyethyl group, fluorine, and the like are introduced in 2'-OH positions of a part of ribose bases may be included.

According to another embodiment, the end of the nucleic acid may be modified by at least one selected from the group consisting of cholesterol, tocopherol, and C10-C24 fatty acid. For example, for siRNA, 5' end or 3' end, or both ends of sense and/or antisense strand may be modified, and preferably, the end of sense strand may be modified.

The cholesterol, tocopherol and fatty acid may include analogues, derivatives and metabolites thereof.

The siRNA refers to duplex RNA or single strand RNA having a double stranded form in the single strand RNA, which may reduce or inhibit the expression of a target gene by mediating degradation of mRNA complementary to the sequence of siRNA if siRNA exists in the same cell as the target gene does. The bond between the double strands is made by hydrogen bond between nucleotides, not all nucleotides in the double strands should be complementarily bound with the corresponding nucleotides, and both strands may be separated or may not be separated. According to one embodiment, the length of the siRNA may be about 15~60 nucleotides (it means the number of nucleotides of one of double stranded RNA, i.e., the number of base pairs, and in the case of a single stranded RNA, it means the length of double strands in the single stranded RNA), specifically about 15~30 nucleotides, and more specifically about 19~25 nucleotides.

According to one embodiment, the double stranded siRNA may have overhang of 1-5 nucleotides at 3' or 5' end or both ends. According to another embodiment, it may be blunt without overhang at both ends. Specifically, it may be siRNA disclosed in US20020086356 and

US7056704.

According to one embodiment, siRNA may have a symmetrical structure with the same lengths of two strands, or it may have a non-symmetrical structure with one strand shorter than the other strand. Specifically, it may be a non-symmetrical siRNA (small interfering RNA) molecule of double strands consisting of 19~21 nucleotide (nt) antisense; and 15~19nt sense having a sequence complementary to the antisense, wherein 5'end of the antisense is blunt end, and the 3'end of the antisense has 1-5 nucleotide overhang. Specifically, it may be siRNA disclosed in WO09/078685.

The anionic drug of the present invention may be included in the content of 0.001 to 10 wt%, specifically 0.01 to 5 wt%, based on the total weight of the composition. If the content is less than 0.001 wt%, the amount of delivery system is too large compared to the drug, and thus, side effect may be caused by delivery system, and if it exceeds 10 wt%, the size of micelle may be too large to decrease stability of the micelle and increase loss rate during filter sterilization. According to one embodiment, the cationic lipid forms a complex with the anionic drug by electrostatic interactions, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer. The cationic lipid may include any lipid capable of forming a complex with the anionic drug by electrostatic interactions, and specific example thereof may include N,N-dioleoyl-N,N-dimethylammoniumchloride (DODAC), N,N-distearyl-N,N-dimethylammoniumbromide (DDAB), N-(1-(2,3-dioleoyloxy)propyl)-N,N,N-trimethylammoniumchloride (DOTAP), N,N-dimethyl-(2,3-dioleoyloxy)propylamine (DODMA), 1,2-diacyl-3-trimethylammonium-propane (TAP), 1,2-diacyl-3-dimethylammonium-propane (DAP), 3 β -[N-(N',N',N'-trimethylaminoethane)carbamoyl]cholesterol (TC-cholesterol), 3 β -[N-(N',N'-dimethylaminoethane)carbamoyl]cholesterol (DC-cholesterol), 3 β -[N-(N'-monomethylaminoethane)carbamoyl]cholesterol (MC-cholesterol), 3 β -[N-(aminoethane)carbamoyl]cholesterol (AC-cholesterol), cholesteryloxypropane-1-amine (COPA), N-(N'-aminoethane)carbamoylpropanoic tocopherol (AC-tocopherol), N-(N'-methylaminoethane)carbamoylpropanoic tocopherol (MC-tocopherol), and a combination thereof. Specifically, to decrease toxicity induced by cationic lipid, it may be preferable to use less polycationic lipid having high charge density, and more specifically, one

functional group capable of exhibiting positive charge in the molecule in an aqueous solution may be included. Specific example of the cationic lipid may include 3β -[N-(N',N',N'-trimethylaminoethane)carbamoyl]cholesterol (TC-cholesterol), 3β [N-(N',N'-dimethylaminoethane)carbamoyl]cholesterol (DC-cholesterol), 3β [N-(N'-monomethylaminoethane)carbamoyl]cholesterol (MC-cholesterol), 3β [N-(aminoethane)carbamoyl]cholesterol (AC-cholesterol), N-(1-(2,3-dioleoyloxy)propyl)-N,N,N-trimethylammoniumchloride (DOTAP), N,N-dimethyl-(2,3-dioleoyloxy)propylamine (DODMA), N,N,N-trimethyl-(2,3-dioleoyloxy)propylamine (DOTMA), and a combination thereof.

The cationic lipid may be included in the content of 0.01 to 50 wt%, specifically 0.1 to 10 wt%, based on the total weight of the composition. If the content is less than 0.01 wt%, it may not be sufficient to form a complex with the anionic drug, and if it exceeds 50 wt%, the size of micelle may be too large to decrease stability of the micelle and increase loss rate during filter sterilization.

The cationic lipid binds with the anionic drug by electrostatic interactions so as to form a complex with the anionic drug. According to one embodiment, the ratio of quantity of electric charge of the anionic drug (N) and the cationic lipid (P) (N/P: the ratio of the negative electric charge of the anionic drug to the positive electric charge of the cationic lipid) is 0.1 to 128, specifically 0.5 to 32, more specifically 1 to 16. If the ratio (N/P) is less than 0.1, it may be difficult to form a complex including a sufficient amount of anionic drug. On the other hand, if the ratio (N/P) exceeds 128, toxicity may be induced.

According to one embodiment, the amphiphilic block copolymer may be an A-B type block copolymer including a hydrophilic A block and a hydrophobic B block. The A-B type block copolymer forms a core-shell type polymeric micelle in an aqueous solution, wherein the hydrophobic B block forms a core and the hydrophilic A block forms a shell.

According to one embodiment, the hydrophilic A block may be at least one selected from the group consisting of polyalkyleneglycol, polyvinyl alcohol, polyvinyl pyrrolidone, polyacrylamide, and a derivative thereof. More specifically, the hydrophilic A block may be at least one selected from the group consisting of monomethoxy polyethylene glycol, monoacetoxy polyethylene glycol, polyethylene glycol, a copolymer of polyethylene and propylene glycol,

and polyvinyl pyrrolidone. According to another embodiment, the hydrophilic A block may have a number average molecular weight of 200 to 50,000 Dalton, specifically 1,000 to 20,000 Dalton, more specifically 1,000 to 5,000 Dalton.

And, if necessary, a functional group or a ligand that may bind to a specific tissue or cell, or a functional group capable of promoting intracellular delivery may be chemically conjugated to the end of the hydrophilic A block so as to control the distribution of the polymeric micelle delivery system in the body or increase the efficiency of the intracellular delivery of polymeric micelle delivery system. The functional group or ligand may include monosaccharide, polysaccharide, vitamins, peptides, proteins, an antibody to a cell surface receptor, and a combination thereof. More specific examples thereof may include anisamide, vitamin B9 (folic acid), vitamin B12, vitamin A, galatose, lactose, mannose, hyaluronic acid, RGD peptide, NGR peptide, transferrin, an antibody to a transferring receptor, and a combination thereof.

The hydrophobic B block is a polymer having excellent biocompatibility and biodegradability, and it may be at least one selected from the group consisting of polyester, polyanhydride, polyamino acid, polyorthoester, and polyphosphazine. More specific examples thereof may include polylactide, polyglycolide, polycaprolactone, polydioxane-2-one, a copolymer of polylactide and glycolide, a copolymer of polylactide and polydioxane-2-one, a copolymer of polylactide and polycaprolactone, a copolymer of polyglycolide and polycaprolactone, and a combination thereof. According to one embodiment, the hydrophobic B block may have a number average molecular weight of 50 to 50,000 Dalton, specifically 200 to 20,000 Dalton, more specifically 1,000 to 5,000 Dalton. And, to increase hydrophobicity of the hydrophobic block for improving the stability of the micelle, tocopherol, cholesterol, or C10-C24 fatty acid may be chemically conjugated to a hydroxyl group of the hydrophobic block end.

The amphiphilic block copolymer comprising the hydrophilic block (A) and the hydrophobic block (B) may be included in the content of 40 to 99.98 wt%, specifically 85 to 99.8 wt%, more specifically 90 to 99.8 wt%, based on the total dry weight of the composition. If the content of the amphiphilic block copolymer is less than 40 wt%, the size of the micelle may become so large that the stability of the micelle may be decreased and the loss during filter sterilization may be increased, and if it exceeds 99.98wt%, the content of anionic drug that can

be incorporated may become too small.

According to another embodiment, the amphiphilic block copolymer may include 40 to 70 wt% of the hydrophilic block (A), specifically 50 to 60 wt% of the hydrophilic block (A), based on the weight of the copolymer. If the ratio of the hydrophilic block (A) is less than 40 wt%, solubility of the polymer in water is low, and thus it may be difficult to form a micelle. On the other hand, if it exceeds 70 wt%, hydrophilicity may be too high and thus stability of the polymeric micelle is low, and it may be difficult to solubilize a complex of the anionic drug and the cationic lipid.

According to one embodiment, the amphiphilic block copolymer allows enclosure of the complex of the anionic drug and the cationic lipid in the micelle structure in an aqueous solution, wherein the ratio of the weight of the complex of the anionic drug and the cationic lipid (a) to the weight of the amphiphilic block copolymer (b) [$a/b \times 100$; (the weight of the anionic drug + the weight of the cationic lipid)/the weight of the amphiphilic block copolymer $\times 100$] may be 0.001 to 100 wt%, specifically 0.01 to 50 wt%, more specifically 0.1 to 10%. If the weight ratio is less than 0.001 wt%, the content of the complex of the anionic drug and the cationic lipid may become too low, and thus it may be difficult to satisfy effective content of the anionic drug, and if it exceeds 100 wt%, a micelle structure of appropriate size may not be formed considering the molecular weight of the amphiphilic block copolymer and the amount of the complex of the anionic drug and the lipid.

According to one embodiment, the pharmaceutical composition of the present invention may further comprise a fusogenic lipid in the content of 0.01 to 50 wt%, specifically 0.1 to 10 wt%, based on the total weight of the composition, in order to increase intracellular delivery efficiency of the anionic drug.

The fusogenic lipid form a complex with the anionic drug, the cationic lipid by the hydrophobic interactions while mixing the anionic drug with the cationic lipid, and the complex comprising the fusogenic lipid is entrapped in the micelle structure of the amphiphilic block copolymer. According to one embodiment, the fusogenic lipid may be phospholipid, cholesterol, tocopherol, or a combination thereof.

Specifically, the phospholipid may be selected from phosphatidylethanolamin (PE), phosphatidylcholine (PC), phosphatidic acid, or a combination thereof. The

phosphatidylethanolamin (PE), phosphatidylcholine (PC) and the phosphatidic acid may be bound to one or two C10-24 fatty acid. The cholesterol and tocopherol may include analogues, derivative, and metabolites thereof.

Specifically, the fusogenic lipid may include dilauroyl phosphatidylethanolamine, dimyristoyl phosphatidylethanolamine, dipalmitoyl phosphatidylethanolamine, distearoyl phosphatidylethanolamine, dioleoyl phosphatidylethanolamine, dilinoleoyl phosphatidylethanolamine, 1-palmitoyl-2-oleoyl phosphatidylethanolamine, 1,2-diphytanoyl-3-sn-phosphatidylethanolamine, dilauroyl phosphatidylcholine, dimyristoyl phosphatidylcholine, dipalmitoyl phosphatidylcholine, distearoyl phosphatidylcholine, dioleoyl phosphatidylcholine, dilinoleoyl phosphatidylcholine, 1-palmitoyl-2-oleoyl phosphatidylcholine, 1,2-diphytanoyl-3-sn-phosphatidylcholine, dilauroyl phosphatidic acid, dimyristoyl phosphatidic acid, dipalmitoyl phosphatidic acid, distearoyl phosphatidic acid, dioleoyl phosphatidic acid, dilinoleoyl phosphatidic acid, 1-palmitoyl-2-oleoyl phosphatidic acid, 1,2-diphytanoyl-3-sn-phosphatidic acid, cholesterol, tocopherol, and a combination thereof.

According to preferred embodiment, the fusogenic lipid may include dioleoyl phosphatidylethanolamine (DOPE), 1,2-dipalmitoleoyl-sn-glycero-3-phosphocholine (DPPC), 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC), 1,2-dipalmitoleoyl-sn-glycero-3-phosphoethanolamine (DPPE), and a combination thereof.

The present invention also provides a method of preparing a pharmaceutical composition comprising an amphiphilic diblock copolymer micelle containing anionic drug.

According to one embodiment, the method of preparing a composition comprising an anionic drug, a cationic lipid, and an amphiphilic block copolymer comprises:

- (a) dissolving the anionic drug and the cationic lipid in a water-miscible organic solvent or a mixed solvent of an aqueous solution and an organic solvent so as to separate the phases;
- (b) separating the organic solvent layer of (a);
- (c) mixing the organic solvent of (b) with the amphiphilic block copolymer and removing the organic solvent; and
- (d) adding an aqueous solution to the mixture from which the organic solvent is removed so as to form a micelle.

In the step (a), the anionic drug and the cationic lipid are mixed in a water-miscible

organic solvent, or a mixed solvent of an aqueous solution and an organic solvent to form a complex. Specifically, the water-miscible organic solvent may include acetone, ethanol, methanol, acetic acid, and a combination thereof, and the organic solvent of the mixed solvent may include ethyl acetate, acetonitrile, methylene chloride, chloroform, dioxane, and a combination thereof. The aqueous solution may include distilled water, water for injection, and a buffer solution. The amount of the complex of the anionic drug and the cationic lipid dissolved in the solvent may be 0.1 ~ 100 wt%, specifically 0.1~10 wt%, more specifically 0.1 ~ 1 wt%, based on the amount of the used solvent. If the amount is 100 wt% or more, yield may be rapidly decreased when the complex of the anionic drug and the cationic lipid is extracted with an organic solvent in the step (b) below.

In the step (b), the complex of the anionic drug and the cationic lipid is recovered by phase separation. An aqueous solution and an organic solvent may be added to the solvent of the step (a) to induce phase separation. And, to shorten the phase separation time, a centrifugation process may be added.

In the step (c), an amphiphilic block copolymer is added to the extracted organic solvent and mixed, and then, the organic solvent is removed by evaporation.

In the step (d), the complex of the anionic drug and the cationic lipid is entrapped in the micelle structure of the amphiphilic block copolymer by dissolving the remaining mixture with an aqueous solution. The aqueous solution may be distilled water, water for injection, or a buffer solution, and the amount may be such that the concentration of the amphiphilic block copolymer may become 10 to 300 mg/mL. If the concentration of the amphiphilic block copolymer is less than 10 mg/mL, the volume of the aqueous solution may become too large thus rendering it difficult to handle during the preparation process, and if it exceeds 300 mg/mL, the viscosity of the aqueous solution may be too high thus rendering it difficult to prepare a micelle.

According to yet another embodiment, a method of preparing a composition for delivery of an anionic drug comprising an anionic drug, a cationic lipid, and an amphiphilic block copolymer comprises:

(a') dissolving the anionic drug, the cationic lipid and the amphiphilic block copolymer in a water-miscible organic solvent or a mixed solvent of an aqueous solution and an organic

solvent;

(b') removing the organic solvent of (a'); and

(c') adding an aqueous solution to the mixture of (b') so as to form a micelle.

In the step (a'), the anionic drug, the cationic lipid, and the amphiphilic block copolymer are mixed in a water-miscible organic solvent, or a mixed solvent of an aqueous solution and an organic solvent to form a complex. Specifically, the water-miscible organic solvent may include acetone, ethanol, methanol, acetic acid, and a combination thereof, and the organic solvent of the mixed solvent may include ethyl acetate, acetonitrile, methylene chloride, chloroform, dioxane, and a combination thereof. The aqueous solution may include distilled water, water for injection, and a buffer solution.

In the step (b'), the organic solvent is removed by evaporation.

In the step (c'), the remaining mixture is dissolved in an aqueous solution, thereby enclosing the complex of the complex of the anionic drug and the cationic lipid in the micelle structure of the amphiphilic block copolymer. The kind and the amount of the aqueous solution are as described above.

According to yet another embodiment, for a composition comprising a fusogenic lipid, the fusogenic lipid may be added together when adding the amphiphilic block copolymer for forming a micelle, and for example, it may be added in the step (c) or (a').

According to yet another embodiment, the method may further comprise (e) adding assistant material for freeze drying, after the step (d) of (c').

According to one embodiment, the method may further comprise sterilizing the polymeric micelle aqueous solution obtained in the step (d) or (c') with a sterilization filter, before the (e) freeze drying.

According to one embodiment, the assistant material for freeze drying may include lactose, mannitol, sorbitol, sucrose, and a combination thereof. The assistant material for freeze drying is added to allow the freeze dried composition to maintain a cake form. According to another embodiment, the content of the assistant material for freeze drying may be 1 to 90 wt%, specifically 10 to 60 wt%, based on the total dry weight of the composition.

According to one embodiment, the amphiphilic block copolymer micelle composition containing an anionic drug may be prepared in the form of an aqueous solution, powder or a

tablet. According to another embodiment, the composition may be prepared for injection. For example, the freeze dried composition may be reconstituted with distilled water for injection, a 0.9% saline solution, a 5% dextrose aqueous solution, and the like.

The micelle formed according to the preparation method of the present invention is stable in blood, and has the particle size of 10 to 200 nm, specifically 10 to 150 nm.

The pharmaceutical composition containing an anionic drug of the present invention may be administered in the route of blood vessel, muscle, subcutaneous, oral, bone, transdermal or local tissue, and the like, and it may be formulated in various forms such as a solution, a suspension for injection, a tablet, or a capsule, and the like.

The pharmaceutical composition containing an anionic drug of the present invention may increase stability of the anionic drug in blood or in body fluid by isolating the anionic drug from outside using the cationic lipid and the amphiphilic block polymer. And, the composition of the present invention may effectively deliver the anionic drug in the cell. And, the amphiphilic polymer has excellent biodegradability and biocompatibility.

□Brief Description of the Drawings□

Fig. 1. is a schematic diagram of the pharmaceutical composition containing an anionic drug according to one embodiment of the present invention.

Fig. 2 is an NMR measurement result of AC-tocopherol prepared by the preparation method according to one embodiment of the present invention.

Fig. 3 is an NMR measurement result of MC-tocopherol prepared by the preparation method according to one embodiment of the present invention.

Fig. 4 is an NMR measurement result of mPEG-PLA block copolymer polymerized by the preparation method according to Example 3 of the present invention.

Fig. 5 is an NMR measurement result of mPEG-PLA block copolymer polymerized by the preparation method according to Example 4 of the present invention.

Fig. 6 is an NMR measurement result of mPEG-PLA-tocopherol polymerized by the preparation method according to Example 5 of the present invention.

Fig. 7 is an NMR measurement result of mPEG-PLA-tocopherol polymerized by the preparation method according to Example 6 of the present invention.

Fig. 8 is an NMR measurement result of anisamide-PEG-PLA polymerized by the preparation method according to one embodiment of the present invention.

□ Examples □

Hereinafter, the present invention will be explained in detail with reference to the following Examples, however these Examples are only to illustrate the invention and the scope of the invention is not limited thereto in any manner.

[Example 1] Synthesis of AC-cholesterol(3β[N-(aminoethane)carbamoyl]cholesterol)

To synthesize AC-cholesterol, cholesteryl chloroformate (Sigma-Aldrich) and ethylenediamine (Sigma-Aldrich) were reacted as follows.

1g (2.23mmol) of cholesteryl chloroformate was dissolved in 20ml of chloroform, 20 equivalents of ethylenediamine was diluted with 30ml of chloroform in a separate reaction vessel, and the temperature was maintained at 4℃. The cholesteryl chloroformate solution was slowly introduced in the reaction vessel containing ethylenediamine, and then, the mixture was reacted at room temperature for 3 hours. After the reaction was completed, the solvent was removed using a rotary evaporator (Buchi, R-2055), and the residue was dissolved again in a small amount of chloroform, and then, extracted with a NaCl saturated solution and NaCO₃ to recover a chloroform layer.

And then, the solvent was removed with a rotary evaporator, and the residue was dissolved in chloroform, and then, silica-gel chromatography was conducted to separate. To a fraction eluted with chloroform:methanol=9:1(v/v), a hydrochloric acid solution was added in 50 equivalents of cholesteryl chloroformate, and methanol was gradually added until a single phase was formed so as to form AC-cholesterol hydrochloride.

The solvent was completely removed by heating and distillation under reduced pressure with a rotary evaporator. The AC-cholesterol hydrochloride was dissolved in methanol of 60℃, and then, cooled to 4℃ to obtain recrystal. The yield was about 53%. Synthesis and purity of AC-cholesterol were confirmed by ¹H-NMR, and the result is shown in Fig. 2. The purity was 99% or more.

[Example 2] Synthesis of MC-cholesterol(3 β [N-(N'-monomethylaminoethane)carbamoyl]cholesterol)

MC-cholesterol was synthesized and purified by the same method as Example 1, except that N-methylethylenediamine (Sigma-Aldrich) was used in 10 equivalents of cholesteryl chloroformate instead of ethylenediamine. The yield was 62%. Synthesis and purity of AC-cholesterol were confirmed by $^1\text{H-NMR}$, and the result is shown in Fig. 3. The purity was 99% or more.

[Example 3] Polymerization of mPEG-PLA (monomethoxy ethylene glycol-poly lactide) block copolymer (A-B) (molecular weight 2,000-1,750 Dalton)

5g of monomethoxy polyethylene glycol (molecular weight 2,000 Dalton or less, NOF corporation) was added to a 100ml two-necked round bottom flask, and heated to 100 $^{\circ}\text{C}$ under reduced pressure (1mmHg) for 3 hours to dehydrate. Dry nitrogen was filled in the reaction flask, and a reaction catalyst of stannous octoate ($\text{Sn}(\text{Oct})_2$, Sigma-Aldrich) was injected in the amount of 0.1wt% of lactide (5 mg). The reaction mixture was agitated for 30 minutes, and pressure was reduced to 1mmHg at 110 $^{\circ}\text{C}$ for 1 hour to remove toluene which is a solvent dissolving the catalyst. Purified lactide (5g, Purac) was added, and the mixture was heated to 130 $^{\circ}\text{C}$ for 12 hours. The formed polymer was dissolved in ethanol, and diethylether was added to precipitate a polymer. The precipitated polymer was dried in a vacuum oven for 48 hours.

The obtained mPEG-PLA has number average molecular weight of 2,000-1,750 Dalton, and it was confirmed to be of A-B type by $^1\text{H-NMR}$ in Fig. 4.

[Example 4] Polymerization of mPEG-PLA (monomethoxy polyethylene glycol-poly lactide) block copolymer (A-B) (molecular weight 5,000-4,000 Dalton)

A mPEG-PLA block copolymer having number average molecular weight of 5,000-4,000 Dalton was synthesized by the same method as Example 3, using monomethoxy polyethylene glycol (molecular weight 5,000 Dalton or less, NOF corporation). The $^1\text{H-NMR}$ measurement results of the obtained mPEG-PLA block copolymer is shown in Fig. 5. As shown in Fig. 5, it is confirmed that the prepared mPEG-PLA block copolymer is of A-B type.

[Example 5] Polymerization of mPEG-PLA-tocopherol (molecular weight 2,000-1,750-530 Dalton)

200ml of acetonitrile (CAN) was used as a reaction solvent, and 26.4 mmol of mPEG-PLA of Example 3 with number average molecular weight of 2,000-1,750 Dalton and 31.68mmol of tocopherol succinate (Sigma-Aldrich) as reactants, and 31.68mmol of dicyclohexyl carbodiimide (DCC, Sigma-Aldrich) and 3.168mmol of dimethylaminopyridine (DAMP, Sigma-Aldrich) as catalysts were introduced to synthesize at room temperature for 24 hours. The acetonitrile solution in which the reaction product was dissolved was filtered with a glass filter to remove dicyclohexylcarburea (DCU) produced during the reaction.

As a primary purification, the filtered acetonitrile solution was precipitated in a cool mixed solvent of diethylether:hexane=3:7(v/v) to recrystallize a polymer. The obtained polymer was dissolved again in an acetonitrile solution and precipitated in a mixed solvent of diethylether:hexane=3:7(v/v) to conduct a secondary purification. The purified polymer was vacuum dried to obtain white powder particles. In the ¹H-NMR analysis of Fig. 6, purity was 97% or more, and yield was 92.7%.

[Example 6] Polymerization of mPEG-PLA-tocopherol (molecular weight 5,000-4,000-530 Dalton)

A mPEG-PLA-tocopherol was polymerized by the same method as Example 5, using mPEG-PLA of Example 4 with number average molecular weight of 5,000-4,000 Dalton. In the ¹H-NMR analysis of Fig. 7, purity was 97% or more, and the yield was 94.2%.

[Example 7] Polymerization of Anisamide-PEG-PLA

0.1 g (660 μ mol) of anisic acid (4-methoxybenzoic acid, Sigma-Aldrich), 0.146g (710 μ mol) of dicyclohexylcarbodiimide (Sigma-Aldrich), and 0.081g (710 μ mol) of N-hydroxysuccinimide (NHS, Sigma-Aldrich) were dissolved in a mixed solvent of acetonitrile:dimethylformamide (DMF)=2:1(v/v) and reacted for 24 hours to synthesize anisic acid-NHS ester (AA-NHS), and then, reaction by product of dicyclohexylcarburea was filtered to remove. 0.519g(260 μ mol) of H₂N-PEG-OH (Mn=2,000, NOF corporation) was dissolved

in 2ml of acetonitrile and 1.5 equivalents of AA-NHS was added, and then, the reaction mixture was reacted at room temperature for 24 hours to synthesize anisamide-PEG (AA-PEG). The process of precipitating the reactant in cool diethylether to recrystallize AA-PEG was repeated twice to purify AA-PEG. The process of polymerizing AA-PEG-PLA-tocopherol from AA-PEG was performed by the same method as Examples 5 and 6. In the ^1H -NMR analysis, introduction rate of anisamide was 90.2%, and the result is shown in Fig. 8.

[Example 8] Preparation of siRNA/cationic lipid complex

A siRNA/cationic lipid complex was prepared using Bligh & Dyer extraction method (Bligh, EG., Dyer, WJ, A rapid method of total lipid extraction and purification, Can. J. Biochem. Physiol 37 (1959) 911-937). 5 μg of the siRNA was used, and as the cationic lipid, AC-cholesterol, MC-cholesterol and TC-cholesterol (Sigma Aldrich) of Examples 1 and 2 were respectively used 0, 1, 2, 4, 8, and 16 times of the moles of siRNA phosphate groups (N/P ratio (the ratio of cation of the cationic lipid to the phosphate groups of siRNA)=0, 1, 2, 4, 8 and 16).

GFP siRNA sequence (Dharmacon):

Sense strand: 5'-GCAAGCUGACCCUGAAGUUDTdT-3' (Sequence ID No. 1)

Antisense strand: 5'-AACUUCAGGGUCAGCUUGCdTT-3' (Sequence ID No. 2)

100 μl of the siRNA aqueous solution, 100 μl of the cationic lipid chloroform solution and 120 μl of methanol were mixed in the above N/P ratio to form a monophasic (Bligh & Dyer monophasic), 100 μl of distilled water and 100 μl of chloroform were added to separate the phases. The amount of siRNA in the aqueous solution layer and the chloroform layer were quantified with a Ribogreen reagent (Invitrogen).

[Table 1]

	Ratio of the amount of siRNA existing in each phase to the amount of siRNA introduced after phase shift (%)					
N/P ratio	AC-cholesterol		MC- cholesterol		TC- cholesterol	
	Aqueous phase	organic phase	Aqueous phase	Organic phase	aqueous phase	Organic phase
0	100.8	0	95.4	0	99.1	0

1	37.7	70.9	93.3	0	0	97.7
2	0	100.1	27.5	72.7	0	98.9
4	0	106.1	0	102.2	0	97.9
8	0	105.6	0	102.8	0	96.8
16	0	114.7	0	105.4	0	98.2

Referring to Table 1, it is confirmed that the cationic lipids form a complex with siRNA and the siRNA/cationic lipid complex is phase-shifted to the organic solvent layer.

[Example 9] Preparation of siRNA/AC-cholesterol/mPEG-PLA polymeric micelle

A siRNA/cationic lipid complex was prepared according to the method of Example 8. The ratio of the cation of AC-cholesterol to the phosphate group of siRNA (N/P ratio) was 6. After phase separation, a chloroform layer was separately collected and added to mPEG-PLA of Example 3 such that the ratio of siRNA/AC-cholesterol complex to mPEG-PLA (molecular weight 2,000-1,750 Dalton) may be 0.51 wt%, and then, the mixture was moved into an 1-necked round flask, and distilled under reduced pressure in a rotary evaporator to remove the solvent. 300 μ L of distilled water was added to the flask, and gently shaken to dissolve, thereby preparing a siRNA/AC-cholesterol/mPEG-PLA polymeric micelle delivery system.

[Example 10] Preparation of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle

A siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle delivery system was prepared by the same method of Example 9, except using mPEG-PLA-tocopherol (molecular weight 2,000-1,750-530 Dalton) of Example 5 instead of mPEG-PLA. The ratio of the siRNA/AC-cholesterol complex to mPEG-PLA-tocopherol was 0.51 wt%.

[Example 11] Preparation of siRNA/AC-cholesterol/mPEG-PLA- tocopherol polymeric micelle

To an one-necked round flask, 46 μ g of AC-cholesterol (N/P ratio = 6) and ethanol were introduced and completely dissolved at room temperature, and then, 5 μ g of siRNA of Example 8

was added and mixed. 9 mg of mPEG-PLA-tocopherol (molecular weight 5,000-4,000-530 Dalton) of Example 6 was added thereto, and agitated at 60 °C for 5 minutes. The ratio of the siRNA/AC-cholesterol complex to mPEG-PLA-tocopherol was controlled to 0.57 wt%.

The mixture was distilled under reduced pressure in a rotary evaporator to remove the solvent. 300 µL of distilled water was added to the flask, and gently shaken to dissolve, thereby preparing a siRNA/AC-cholesterol/ mPEG-PLA polymeric micelle delivery system.

[Example 12] Preparation of VEGF siRNA or siRNA-cholesterol/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle

VEGF siRNA of the following Sequence ID Nos. 3 and 4 and VEGF siRNA-cholesterol which has a sequence identical to the above sequence but includes cholesterol covalently bonded at 3'end were purchased from Samchully Pharm., and VEGF siRNA and VEGF siRNA-cholesterol polymeric micelle delivery system was prepared by the same method as Example 11.

VEGF siRNA (Dharmacon):

Sense strand: 5'-GGAGUACCCUGAUGAGAUCdTdT-3' (Sequence ID No. 3),

Antisense strand: 5'-GAUCUCAUCAGGGUACUCCdTdT-3' (Sequence ID No. 4)

[Example 13] Preparation of siRNA/AC-cholesterol/mPEG-PLA-tocopherol/dioleylphosphatidyl-ethanolamine (DOPE) polymeric micelle

In the composition of Example 11, 34µg of DOPE (Avanti polar lipids) was additionally added together with the polymer to prepare a DOPE-containing siRNA polymeric micelle delivery system by the same method as Example 11.

[Experimental Example 1] Measurement of the size of siRNA/cationic lipid/amphiphilic block copolymeric micelle and confirmation of siRNA enclosure

To confirm whether the siRNA/cationic lipid containing amphiphilic block copolymer forms a nanoparticle, the sizes of siRNA/AC-cholesterol/mPEG-PLA polymeric micelle and siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle were measured by DLS

(Dynamic Light Scattering) method and described in Table 2.

A helium-neon laser with an output of 10 mV and wavelength of 638 nm was used as a light source, incident light of 90° was used, and the experiment was conducted at 25°. The measurement and analysis were conducted using an ELS-8000 equipment of Photol Otsuka Electronics Co. Ltd.

[Table 2]

	Kind of polymer	Weight average particle size
Example 9	siRNA/AC-cholesterol/mPEG-PLA	27.6±16.9nm
Example 10	siRNA/AC- cholesterol/mPEG-PLA-tocopherol	26.8±7.2 nm
Example 11	siRNA/AC- cholesterol/mPEG-PLA- tocopherol	54.5±17.0nm
Example 12	VEGF siRNA- cholesterol/AC- cholesterol/mPEG-PLA-tocopherol	60.0±15.4 nm
Example 13	siRNA/AC- cholesterol/mPEG-PLA-tocopherol /DOPE	82.4±28.5 nm

The siRNA was quantified in the prepared siRNA/cationic lipid containing amphiphilic block copolymeric micelle by a modified Bligh & Dyer extraction method.

The polymeric micelle delivery systems prepared in each Example was dissolved in 50 mM sodium phosphate, 75 mM NaCl (pH 7.5), and a Bligh & Dyer monophasic was formed, and then, extracted with 100 mM sodium phosphate, 150 mM NaCl (pH 7.5) to quantify the siRNA of the aqueous solution layer with a Ribogreen reagent (Invitrogen).

As result of measurement, 90% or more of the siRNA amount could be extracted.

[Experimental Example 2] Blood stability measurement of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle

To examine how safely the siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle protects siRNA in blood, half life of siRNA was measured in blood serum. The

polymeric micelle of Example 10 (polymeric micelle 1) and the polymeric micelle of Example 11 (polymeric micelle 2) were cultured at 37°C, in 50% blood serum for the time described in Table 3, and then, the amount of siRNA was quantified to calculate the half life as follows.

To measure the total amount of siRNA of the polymeric micelle, modified Bligh & Dyer method as Experimental Example 1 was performed. The measurement results are described in the following Table 3.

[Table 3]

Time (min)	Non-enclosed siRNA(%)	siRNA(%) of polymeric micelle 1	siRNA(%) of polymeric micelle 2
30	32.4	63.6	92.5
60	29.1	57.6	74.7
120	19.8	46.9	58.1
240	8.8	31.2	47.4

Referring to Table 3, it is confirmed that the half life of non-enclosed siRNA is 28.4 minutes, while the half life of the siRNA enclosed in the polymeric micelle 1 of Example 10 is 126 minutes and the half life of the siRNA enclosed in the polymeric micelle 2 of Example 11 is 192.5 minutes, and that the half lives of siRNAs increased respectively 4.4 times and 6.8 times compared to the non-enclosed siRNA. It can be seen from the Table 3 that siRNA may be stabilized in blood by enclosing siRNA in a polymeric micelle.

[Experimental Example 3] Stability evaluation of siRNA or siRNA-cholesterol/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle to RNase

It was examined how safely a siRNA or siRNA-cholesterol/AC-cholesterol/mPEG-PLA-tocopherol containing composition protects siRNA to RNase. The polymeric micelle of Example 11 (polymeric micelle 2) and the siRNA-cholesterol polymeric micelle of Example 12 (polymeric micelle 3) were cultured with 10U RNase VI (Promega) for the time described in Table 4, and then, the amount of siRNA was quantified by the same method as Experimental Example 1. The measurement result is described in the following Table 4.

[Table 4]

Time (min)	Amount of non-enclosed siRNA(%)	siRNA amount of polymeric micelle 2 (siRNA) (%)	Amount of non-enclosed siRNA-cholesterol (%)	siRNA amount of polymeric micelle 3 (siRNA-cholesterol) (%)
40	0	58.6	3.9	103.0
70	0	53.2	3.7	101.7
130	0	40.3	2.4	103.4

Referring to Table 4, it can be seen that the non-enclosed siRNA was completely degraded within 40 minutes after RNase treatment, while if the siRNA is enclosed in the polymeric micelle, about 40% remained stably even 130 minutes after RNase treatment. Meanwhile, it can be seen that siRNA-cholesterol has slightly higher stability than siRNA in non-enclosed states, and that if the siRNA-cholesterol is enclosed in the polymeric micelle (polymeric micelle 3), stability much increased compared to the siRNA enclosed in the polymeric micelle (polymeric micelle 2). Thus, it can be seen from the Table 4 that siRNA could be stabilized to RNase by enclosing siRNA in the polymeric micelle, and that the effect is more exhibited for siRNA-cholesterol.

[Experimental Example 4] Evaluation of activity of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle (protein level)

An A549 GFP cell line expressing GFP (Green fluorescence protein) [commonly prepared from A549 cell line (ATCC)] was treated with the GFP siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle of Example 10 and 11. And then, intracellular delivery capacity of the polymeric micelle was measured by measuring fluorescence shown by the expression of GFP protein.

The compositional ratio of the GFP siRNA/AC-cholesterol/mPEG-PLA-tocopherol containing composition is as described in the following Table 5.

[Table 5]

Example	composition	N/P Ratio	mPEG-PLA-tocopherol molecular weight	siRNA/AC-cholesterol amount (weight ratio) compared to mPEG-PLA-tocopherol
10	1	6	2,000-1,750-530	0.648
	2	4	2,000-1,750-530	0.669
	3	3	2,000-1,750-530	0.700
11	4	6	5,000-4,000-530	0.648
	5	4	5,000-4,000-530	0.669
	6	3	5,000-4,000-530	0.700

1×10^4 cells were divided on a 96-well cell plate, and after 24 hours, treated with 30 Nm of siRNA in the presence of 10% blood serum for 24 hours, and then, the medium was changed. After 24 hours, GFP fluorescence was measured with an ELISA reader (excitation wavelength: 485/20 nm, emission wavelength: 528/20 nm). The measurement result is shown in the following Table 6. Control was treated with phosphate buffered saline only.

[Table 6]

Example	composition	GFP Fluorescence (%)	Cell viability (%)	GFP fluorescence /cell viability (%)
	Control	98.4	99.8	98.6
10	1	48.1	89.9	53.6
	2	63.4	101.1	62.8
	3	68.2	101.1	67.6
11	4	67.7	90.9	74.5
	5	62.2	96.1	64.8
	6	80.7	95.4	84.6

Table 6 shows results obtained by measuring GFP fluorescence, and then, calculating

cell viability by SRB assay, and dividing the GFP fluorescence value by the cell viability. It can be seen from Table 6 that GFP protein expression was inhibited about 30~40%.

[Experimental Example 5] Evaluation of activity (mRNA level) of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle

For the compositions 1 to 3 of Experimental Example 4, the activity of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle was confirmed at mRNA level. The polymeric micelle was treated under the same conditions as Experimental Example 4, except that the administration concentration of siRNA was varied to 15 nM and 30 nM. Cells were treated with the polymeric micelle, and after 48 hours, GFP mRNA and GAPDH mRNA were subjected to Quantitative RT-PCR to comparatively quantify GFP mRNA. Control was treated with phosphate buffered saline only. The result of quantification is shown in the following Table 7

[Table 7]

Composition	Administration concentration (nM)	GFP mRNA expression (%)
Control	0	100.0%
1	15	40.1%
	30	4.6%
2	15	66.9%
	30	6.1%
3	15	71.2%
	30	10.3%

Table 7 shows the activities of tocopherol polymeric micelle delivery systems examined by the expression amount of mRNA. It can be seen from the Table 7 that the amount of GFP mRNA decreased in proportion to the administration amount, and that GFP mRNA was inhibited 90% or more at 30 nM.

[Experimental Example 6] Activity comparison experiment of siRNA polymeric micelle and lipofectamine

The activity of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle and the activity of lipofectamine (Invitrogen) commercially used for cell delivery of nucleic acid were compared at protein level. The experiment was conducted by the same method as Experimental Example 4 for the composition 1 of Experimental Example 4. Control was treated with phosphate buffered saline only. The results are shown in the following Table 8.

[Table 8]

composition	GFP fluorescence(%)	Cell viability (%)	GFP fluorescence/ cell viability (%)
control	98.4	99.8	98.6
Composition 1 of Experimental Example 4	57.0	99.5	57.3
Lipofectamine	47.9	73.0	65.5

Table 7 shows the results of comparison of activities of siRNA polymeric micelle and lipofectamine examined by the amount of protein expression. It can be seen from the Table 8 that siRNA polymer inhibited expression of GFP protein with the similar level to lipofectamine while exhibiting higher cell viability. This means that siRNA polymeric micelle delivery system has more excellent activity compared to toxicity than lipofectamine.

[Experimental Example 7] In vivo activity of siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle

It was confirmed whether siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle can inhibit target gene VEGF (vascular endothelial growth factor) of used siRNA in the living body.

A nude mouse (provided by Central Lab. Animal Inc.) was subcutaneously injected with A549 lung cancer cell line (ATCC) to prepare a cancer-induced mouse. The cancer model

mouse was intravenously injected with the VEGF siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle of Example 12 at a dose of 1.5 mg/kg, and after 48 hours, cancer tissue was extracted. The extracted cancer tissue was pulverized and the amount of VEGF protein was analyzed by ELISA. The ELISA was conducted according to the instruction of kit manufacturer (R&D systems). As control, saline solution was injected. The results are shown in Table 9.

[Table 9]

Group	Individual	VEGF concentration (pg/ml)	Relative amount (%)	average (%)
Control	#1	820.6	127.5	100.0
	#2	475.0	73.8	
	#3	610.5	94.9	
	#4	668.3	103.8	
VEGF siRNA polymeric micelle	#1	342.7	53.3	57.2
	#2	344.9	53.6	
	#3	356.8	55.4	
	#4	427.5	66.4	

Table 9 shows inhibition rate of target gene in cancer tissue after intravenous injection of siRNA polymeric micelle delivery system in a cancer model mouse. The siRNA polymeric micelle delivery system inhibited the amount of VEGF protein about 43% in the cancer tissue. It can be seen from the Table 9 that systemic delivery of siRNA may be enabled with the siRNA polymeric micelle delivery system.

[Experimental Example 8] In vivo activity of siRNA-cholesterol/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle

The experiment was conducted by the same method as Experimental Example 7, except using VEGF siRNA-cholesterol/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle of Example 12, and then, the concentration of VEGF was analyzed. As control, a saline solution was used. The results are shown in Table 10.

[Table 10]

Group	individual	VEGF concentration (pg/ml)	Relative amount (%)	average (%)
Control	#1	438.6	82.9	100.0
	#2	403.7	76.3	
	#3	745.6	140.9	
siRNA -cholesterol polymeric micelle of Example 12	#1	218.9	41.4	32.0
	#2	173.1	32.7	
	#3	115.3	21.8	

Table 10 shows inhibition rate of target gene in the cancer tissue after intravenous injection of siRNA-cholesterol polymeric micelle delivery system in a cancer model mouse. The siRNA-cholesterol polymeric micelle delivery system inhibited the amount of VEGF protein about 68% in the cancer tissue. It can be seen from the Table 10 that systemic delivery of siRNA may be enabled with the siRNA-cholesterol polymeric micelle delivery system.

[Experimental Example 9] Evaluation of activity (protein level) of siRNA/AC-cholesterol/mPEG-PLA-tocopherol/DOPE polymeric micelle

The effect of addition of DOPE to siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle on the activity was examined. A polymeric micelle comprising DOPE was prepared by the same method as Example 13 with the VEGF siRNA sequence of Example 12. A549 cell lines were respectively treated with the above micelle and the VEGF siRNA/AC-cholesterol/mPEG-PLA-tocopherol polymeric micelle of Example 12 by the same method as Experimental Example 4. The medium was recovered, and the concentration of released VEGF in the medium was measured by the method described in Experimental Example 7, and corrected with respect to control treated with phosphate buffered saline only. The measurement results are shown in the following Table 11.

[Table 11]

	control	siRNA polymeric micelle	DOPE containing siRNA polymeric micelle
VEGF concentration	100%	79.1%	38.8%
siRNA activity (VEGF inhibition rate)	0%	20.9%	61.2%

Table 11 shows quantification of the concentration of VEGF protein released in the medium after treating the siRNA polymeric micelle. It can be seen from the Table 11 that siRNA activity largely increases from 20.9% to 61.2% by adding DOPE to the siRNA polymeric micelle.

CLAIMS:

1. A composition for delivery of an anionic drug comprising
an anionic drug as an active ingredient; a cationic lipid ; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, and
wherein the anionic drug is a nucleic acid,
the cationic lipid is a cationic lipid forming a complex with the nucleic acid by electrostatic interactions,
the amphiphilic block copolymer is an A-B type di-block copolymer comprising a hydrophilic A block and a hydrophobic B block,
wherein the hydrophilic A block is one or more selected from the group consisting of polyalkyleneglycol, polyvinyl alcohol, polyvinyl pyrrolidone, and polyacrylamide, which may be conjugated with a functional group or a ligand that may bind to a specific tissue or cell, or a functional group capable of promoting intracellular delivery, and
the hydrophobic B block is one or more selected from the group consisting of polyester, polyanhydride, polyamino acid, polyorthoester, and polyphosphazine, which may be conjugated to a moiety to increase the hydrophobicity of the hydrophobic block.
2. The composition of claim 1, wherein the nucleic acid is one or more selected from the group consisting of RNA, DNA, siRNA (short interfering RNA), aptamer, antisense ODN (oligodeoxynucleotide), antisense RNA, ribozyme, and DNAzyme.
3. The composition of claim 1, wherein the nucleic acid is modified by modifying at least one end of the nucleic acid with one or more selected from the group consisting of cholesterol, tocopherol, and C10-C24 fatty acid.
4. The composition of claim 1, wherein the cationic lipid is one or more selected from the group consisting of N,N-dioleoyl-N,N-dimethylammoniumchloride (DODAC), N-(1-(2,3-dioleoyloxy)propyl)-N,N,N-trimethylammoniumchloride (DOTAP), N,N-dimethyl-(2,3-dioleoyloxy)propylamine (DODMA), 1,2-diacyl-3-trimethylammonium-propane (TAP), 1,2-diacyl-3-dimethylammonium-propane (DAP), 3β -[N-(N',N',N'-trimethylaminoethane)carbamoyl]cholesterol (TC-cholesterol), 3β [N-(N',N'-dimethylaminoethane)carbamoyl]cholesterol (DC-cholesterol), 3β [N-(N'-

monomethylaminoethane)carbamoyl]cholesterol (MC-cholesterol), 3β [N-(aminoethane)carbamoyl]cholesterol (AC-cholesterol), cholesteryloxypropane-1-amine (COPA), N-(N'-aminoethane)carbamoylpropanoic tocopherol (AC-tocopherol), and N-(N'-methylaminoethane)carbamoylpropanoic tocopherol (MC-tocopherol).

5. The composition of claim 1, wherein the ratio of quantities of electric charges of the anionic drug (N) and the cationic lipid (P) (N/P) is 0.1 to 128.

6. The composition of claim 1, wherein the hydrophilic A block is one or more selected from the group consisting of monomethoxy polyethylene glycol, monoacetoxypolyethylene glycol, polyethylene glycol, a copolymer of polyethylene and propylene glycol, and polyvinyl pyrrolidone, and the hydrophobic B block is one or more selected from the group consisting of polylactide, polyglycolide, polycaprolactone, polydioxane-2-one, a copolymer of polylactide and glycolide, a copolymer of polylactide and polydioxane-2-one, a copolymer of polylactide and polycaprolactone, and a copolymer of polyglycolide and polycaprolactone.

7. The composition of claim 1, wherein the hydrophilic A block has a number average molecular weight of 200 to 50,000 Dalton, and the hydrophobic B block has a number average molecular weight of 50 to 50,000 Dalton.

8. The composition of claim 1, wherein the ratio of the weight of the complex of the anionic drug and the cationic lipid (a) to the weight of the amphiphilic block copolymer (b) ($a/b \times 100$) is 0.001 to 100 wt%.

9. The composition of claim 1, further comprising at least one fusogenic lipid selected from the group consisting of phospholipid, cholesterol, and tocopherol.

10. The composition of claim 9, wherein the phospholipid is one or more selected from the group consisting of phosphatidylethanolamine (PE), phosphatidylcholine (PC), and phosphatidic acid.

11. The composition of claim 9, wherein the fusogenic lipid is one or more selected from the group consisting of dilauroyl phosphatidylethanolamine, dimyristoyl

phosphatidylethanolamine, dipalmitoyl phosphatidylethanolamine, distearoyl phosphatidylethanolamine, dioleoyl phosphatidylethanolamine, dilinoleoyl phosphatidylethanolamine, 1-palmitoyl-2-oleoyl phosphatidylethanolamine, 1,2-diphytanoyl-3-sn-phosphatidylethanolamine, dilauroyl phosphatidylcholine, dimyristoyl phosphatidylcholine, dipalmitoyl phosphatidylcholine, distearoyl phosphatidylcholine, dioleoyl phosphatidylcholine, dilinoleoyl phosphatidylcholine, 1-palmitoyl-2-oleoyl phosphatidylcholine, 1,2-diphytanoyl-3-sn-phosphatidylcholine, dilauroyl phosphatidic acid, dimyristoyl phosphatidic acid, dipalmitoyl phosphatidic acid, distearoyl phosphatidic acid, dioleoyl phosphatidic acid, dilinoleoyl phosphatidic acid, 1-palmitoyl-2-oleoyl phosphatidic acid, 1,2-diphytanoyl-3-sn-phosphatidic acid, cholesterol, and tocopherol.

12. A method of preparing a composition for delivery of an anionic drug comprising an anionic drug, a cationic lipid, and an amphiphilic block copolymer, which method comprises:

(a) dissolving the anionic drug and the cationic lipid in a water-miscible organic solvent or a mixed solvent of an aqueous solution and an organic solvent, to separate the phases;

(b) separating the organic solvent layer of (a);

(c) mixing the organic solvent layer of (b) with the amphiphilic block copolymer and removing the organic solvent; and

(d) adding an aqueous solution to the mixture from which the organic solvent is removed, to form a micelle,

wherein the anionic drug is a nucleic acid,

the cationic lipid is a cationic lipid forming a complex with the nucleic acid by electrostatic interactions,

the amphiphilic block copolymer is an A-B type di-block copolymer comprising a hydrophilic A block and a hydrophobic B block,

wherein the hydrophilic A block is one or more selected from the group consisting of polyalkyleneglycol, polyvinyl alcohol, polyvinyl pyrrolidone, and polyacrylamide, which may be conjugated with a functional group or a ligand that may bind to a specific tissue or cell, or a functional group capable of promoting intracellular delivery, and

the hydrophobic B block is one or more selected from the group consisting of polyester, polyanhydride, polyamino acid, polyorthoester, and polyphosphazine, which may be conjugated to a moiety to increase the hydrophobicity of the hydrophobic block.

13. A method of preparing a composition for delivery of an anionic drug comprising an anionic drug, a cationic lipid, and an amphiphilic block copolymer, which method comprises:

(a') dissolving the anionic drug, the cationic lipid and the amphiphilic block copolymer in a water-miscible organic solvent or a mixed solvent of an aqueous solution and an organic solvent;

(b') removing the organic solvent layer of (a'); and

(c') adding an aqueous solution to the mixture of (b') from which the organic solvent is removed so as to form a micelle,

wherein the anionic drug is a nucleic acid,

the cationic lipid is a cationic lipid forming a complex with the nucleic acid by electrostatic interactions,

the amphiphilic block copolymer is an A-B type di-block copolymer comprising a hydrophilic A block and a hydrophobic B block,

wherein the hydrophilic A block is one or more selected from the group consisting of polyalkyleneglycol, polyvinyl alcohol, polyvinyl pyrrolidone, and polyacrylamide, which may be conjugated with a functional group or a ligand that may bind to a specific tissue or cell, or a functional group capable of promoting intracellular delivery, and

the hydrophobic B block is one or more selected from the group consisting of polyester, polyanhydride, polyamino acid, polyorthoester, and polyphosphazine, which may be conjugated to a moiety to increase the hydrophobicity of the hydrophobic block.

14. The method of claim 12 or claim 13, further comprising:

(e) adding an assistant agent for freeze drying to freeze dry, after Step (d) or (c'), to perform freeze drying.

15. The method of claim 12 or claim 13, further comprising:

adding a fusogenic lipid in Step (c) or (a').

16. The method of claim 12 or claim 13, wherein the cationic lipid is one or more selected from the group consisting of N,N-dioleoyl-N,N-dimethylammoniumchloride (DODAC), N-(1-(2,3-dioleoyloxy)propyl)-N,N,N-trimethylammoniumchloride (DOTAP), N,N-dimethyl-(2,3-dioleoyloxy)propylamine (DODMA), 1,2-diacyl-3-trimethylammonium-

propane (TAP), 1,2-diacyl-3-dimethylammonium-propane (DAP), 3β -[N-(N',N',N'-trimethylaminoethane)carbamoyl]cholesterol (TC-cholesterol), 3β [N-(N',N'-dimethylaminoethane)carbamoyl]cholesterol (DC-cholesterol), 3β [N-(N'-monomethylaminoethane)carbamoyl]cholesterol (MC-cholesterol), 3β [N-(aminoethane)carbamoyl]cholesterol (AC-cholesterol), cholesteryloxypropane-1-amine (COPA), N-(N'-aminoethane)carbamoylpropanoic tocopherol (AC-tocopherol), and N-(N'-methylaminoethane)carbamoylpropanoic tocopherol (MC-tocopherol).

17. The method of claim 12 or claim 13, wherein the ratio of the quantity of electric charge of the anionic drug (N) and the cationic lipid (P) (N/P) is 0.1 to 128.

18. The method of claim 12 or claim 13, wherein the ratio of the weight of the complex of the anionic drug and the cationic lipid (a) to the weight of the amphiphilic block copolymer (b) ($a/b \times 100$) is 0.001 to 100 wt%.

19. A use of a composition for delivery of an anionic drug, wherein the composition comprises:

an anionic drug as an active ingredient; a cationic lipid ; and an amphiphilic block copolymer, wherein the anionic drug forms a complex with the cationic lipid, and the complex is entrapped in the micelle structure of the amphiphilic block copolymer, and

wherein the anionic drug is a nucleic acid,

the cationic lipid is a cationic lipid forming a complex with the nucleic acid by electrostatic interactions,

the amphiphilic block copolymer is an A-B type di-block copolymer comprising a hydrophilic A block and a hydrophobic B block,

wherein the hydrophilic A block is one or more selected from the group consisting of polyalkyleneglycol, polyvinyl alcohol, polyvinyl pyrrolidone, and polyacrylamide, which may be conjugated with a functional group or a ligand that may bind to a specific tissue or cell, or a functional group capable of promoting intracellular delivery, and

the hydrophobic B block is one or more selected from the group consisting of polyester, polyanhydride, polyamino acid, polyorthoester, and polyphosphazine, which may be conjugated to a moiety to increase the hydrophobicity of the hydrophobic block.

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Fig. 2

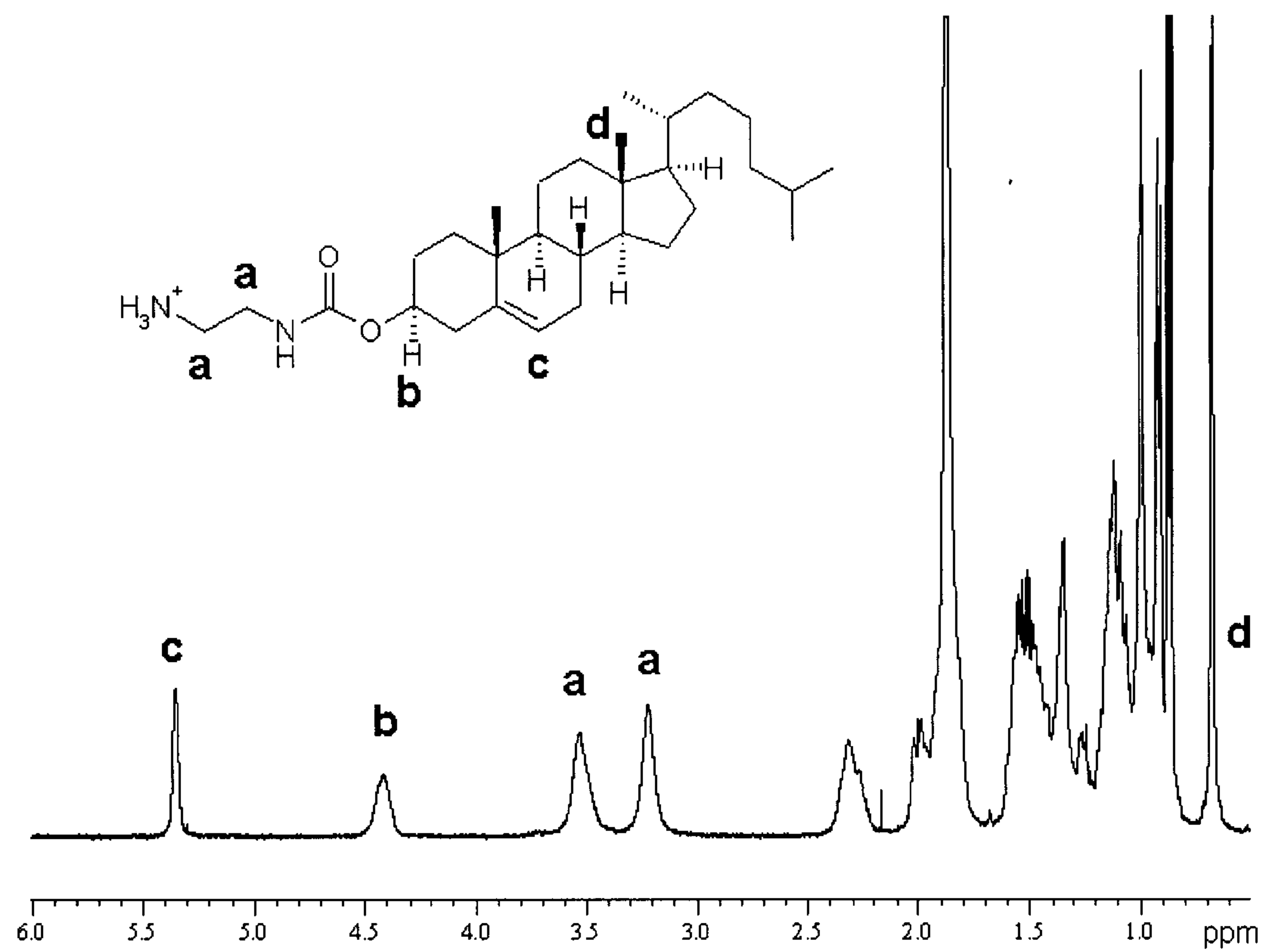


Fig. 3

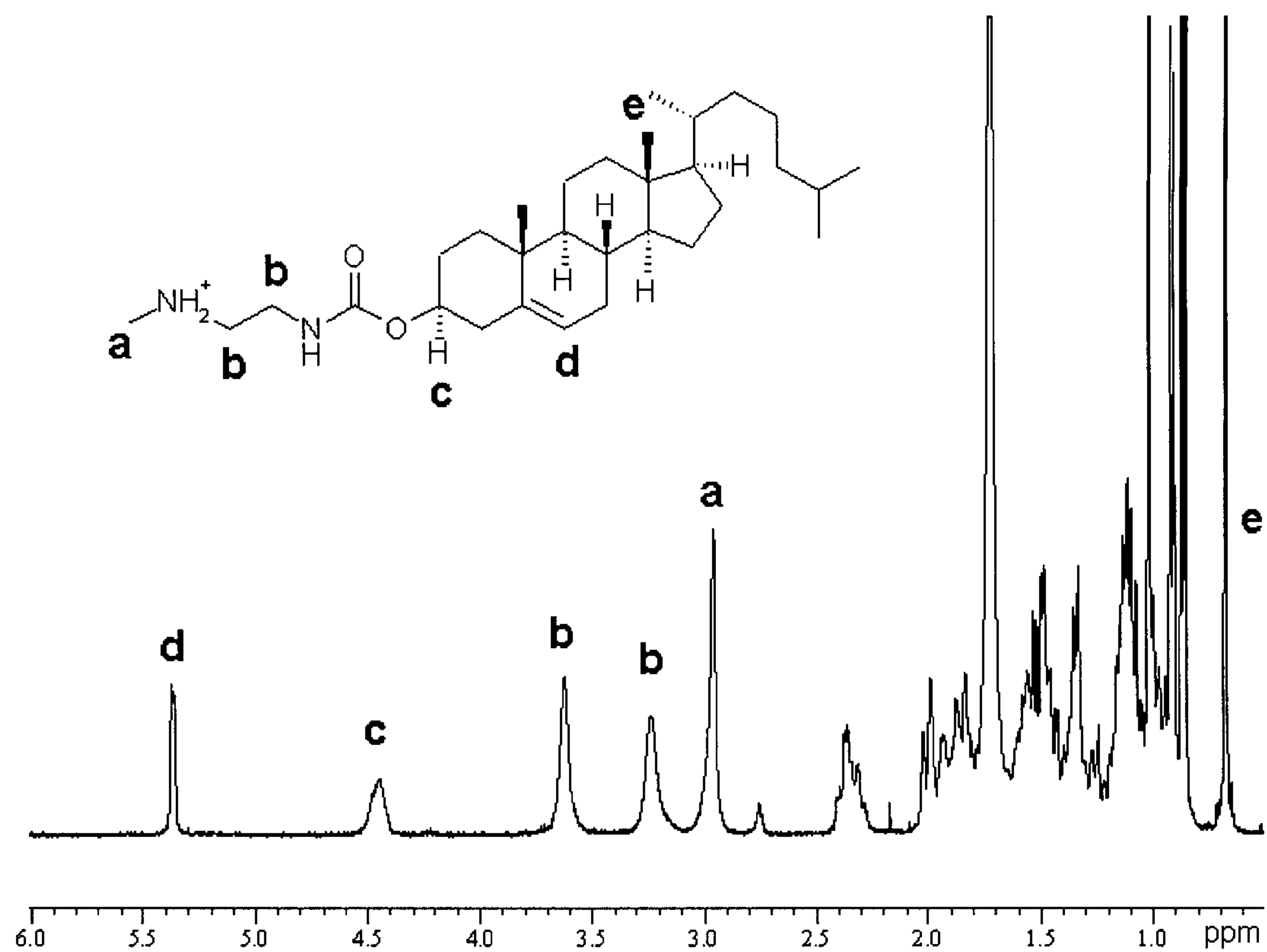


Fig. 4

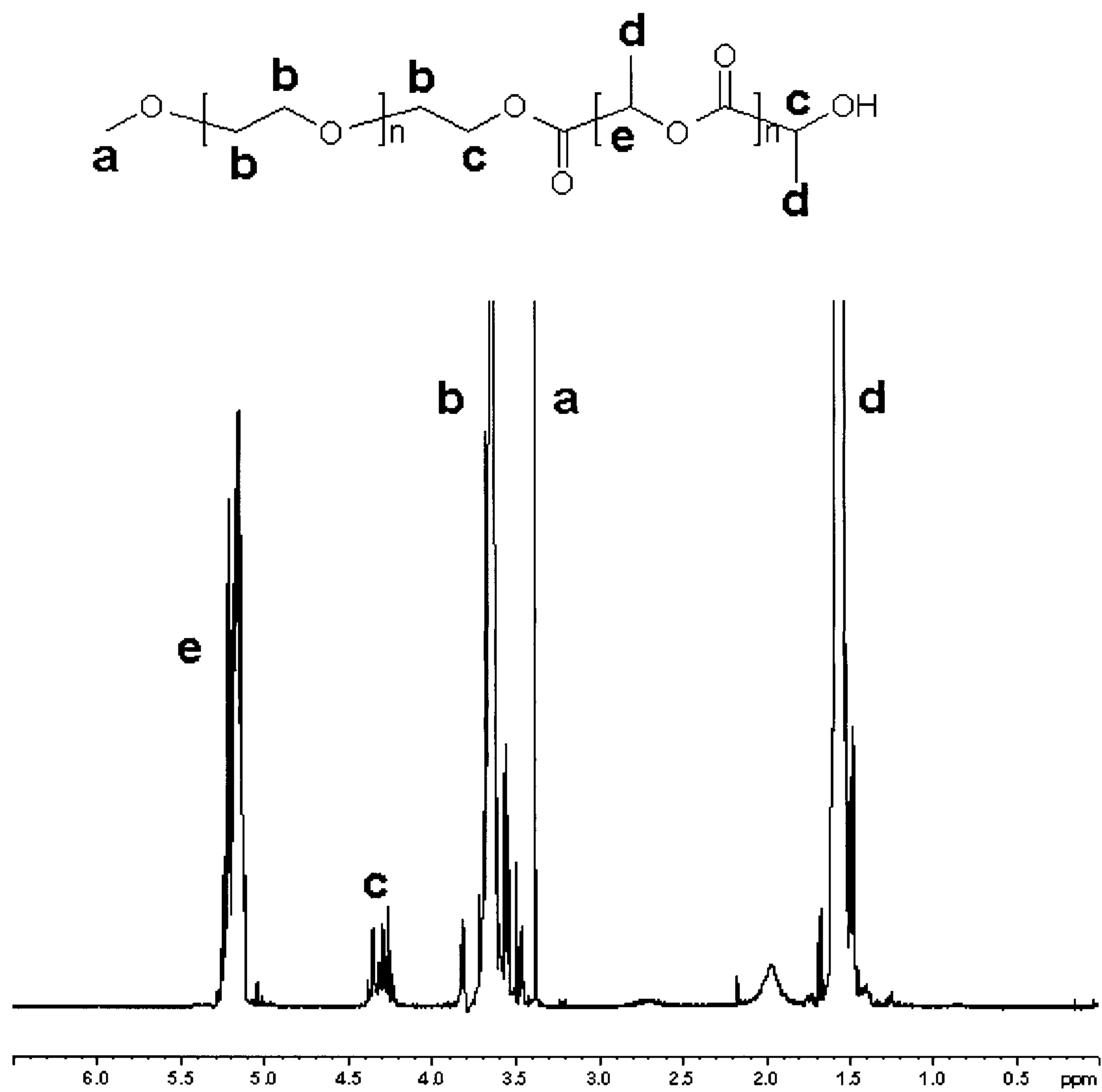


Fig. 5

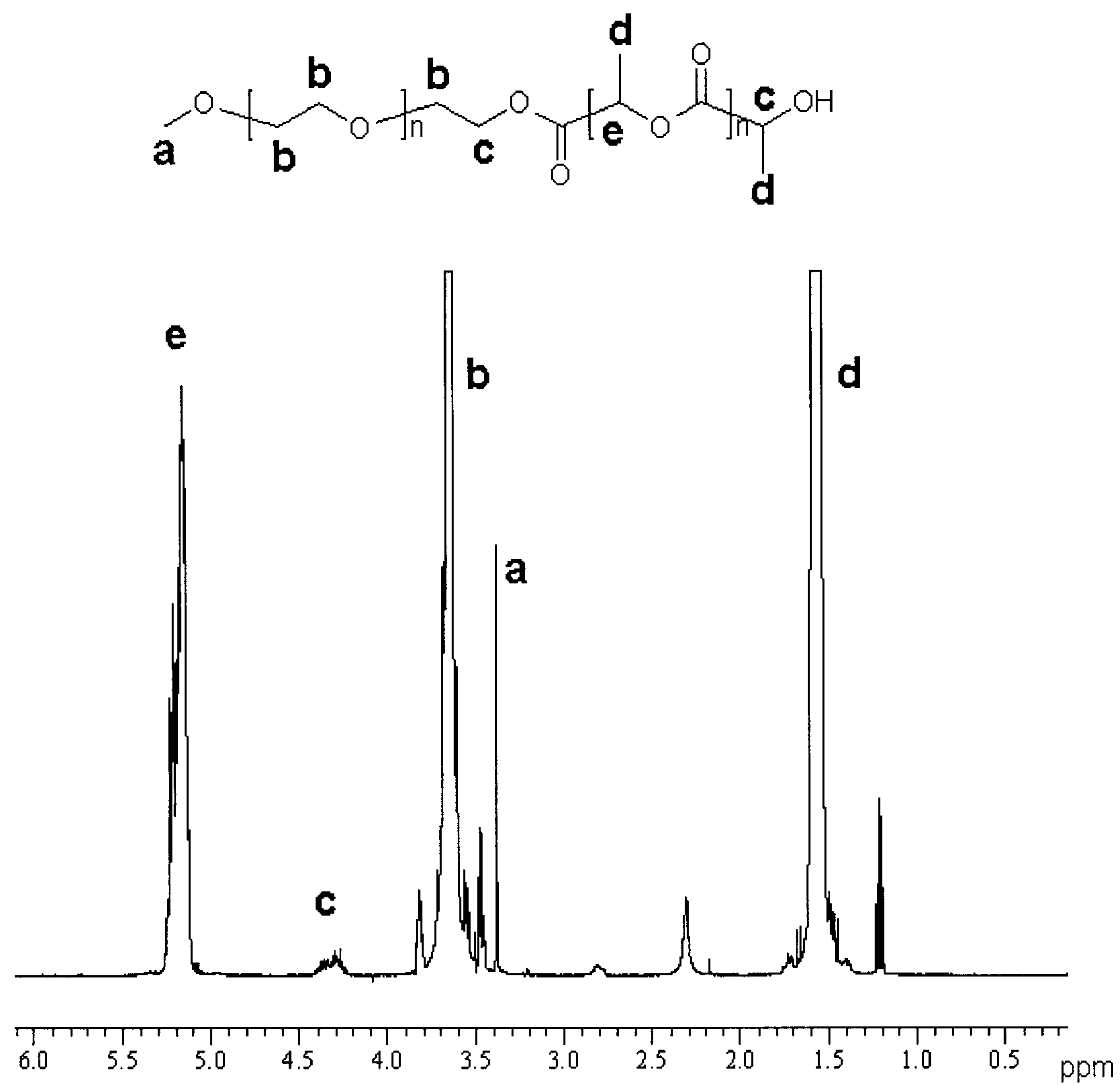


Fig. 6

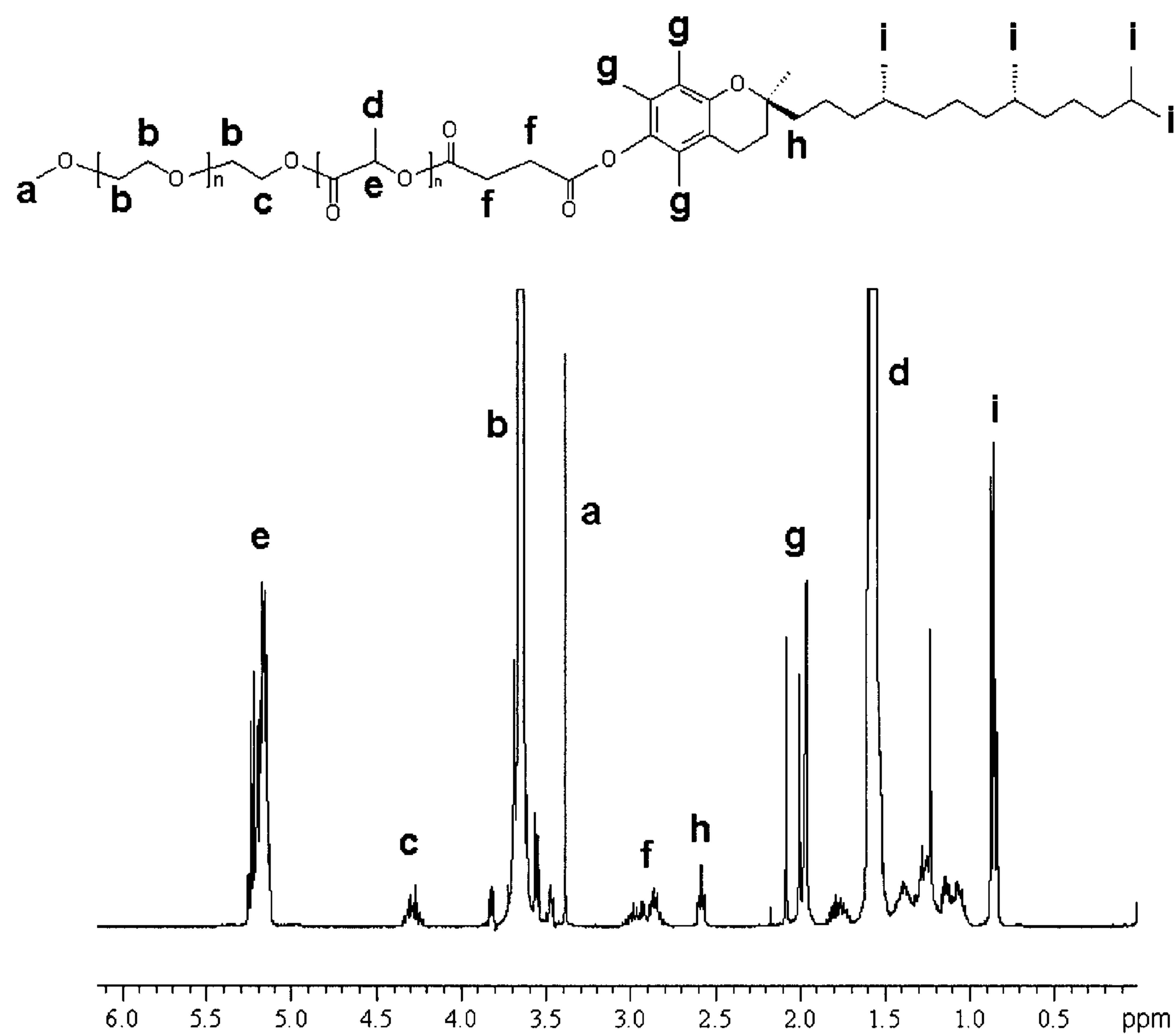


Fig. 7

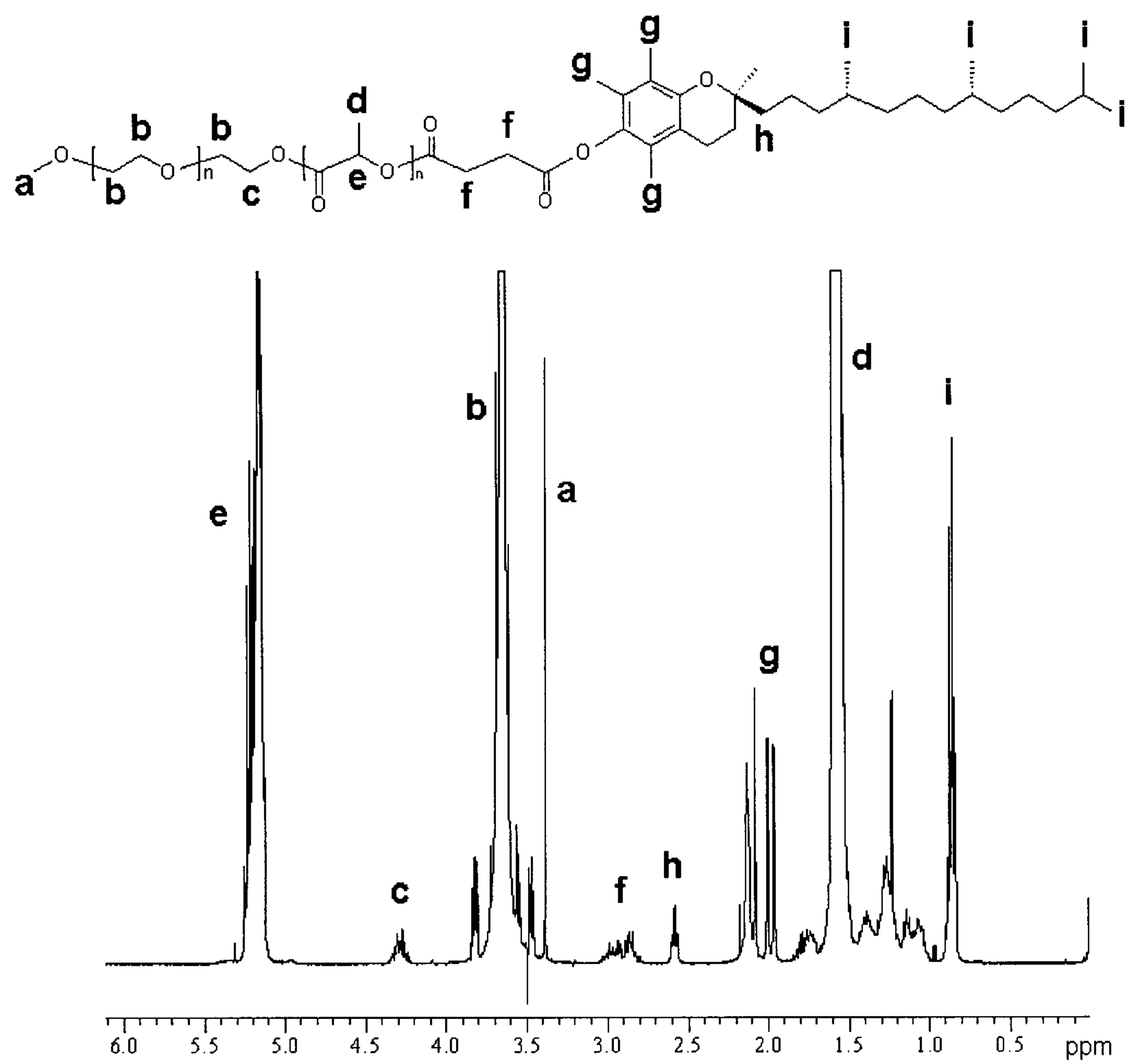


Fig. 8

