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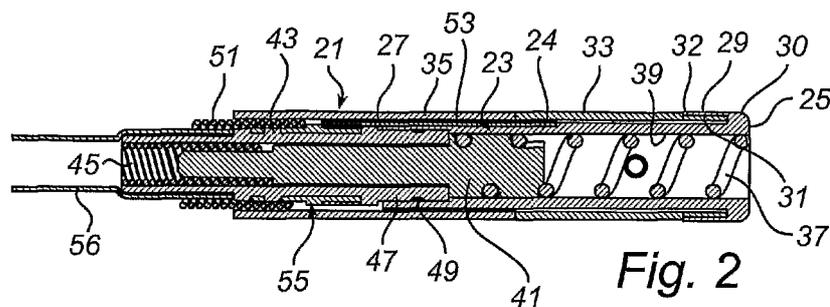
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(54) **Title:** A MEDICAL IMPLANTABLE LEAD WITH, A HEADER AT A DISTAL END AND A MARKER THEREON



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(57) **Abstract:** This invention relates to a medical implantable lead having a proximal end and a distal end, a biostable and biocompatible polymeric header, which is arranged at the distal end and has a first tubular portion, a helical fixation element located within the first tubular portion and being extendable from a distal end of the header, and a radiopaque ring. The header further comprises a second tubular portion, which is arranged coaxially of the first tubular portion and is attached to the first tubular portion at a distal end of the second tubular portion, while having a free proximal end. Thereby the tubular portions form a circumferential pocket, wherein the first tubular portion extends from the proximal end of the header at least to said distal end of the second tubular portion. The radiopaque ring is arranged around the first tubular portion and is received in the circumferential pocket.

**MEDICAL IMPLANTABLE LEAD WITH A HEADER AT A DISTAL END  
AND A MARKER THEREON**

TECHNICAL FIELD

The present invention relates to a medical implantable lead having a header arranged at a distal end thereof and a radiopaque ring arranged at the header.

5

BACKGROUND ART

A lead of the kind mentioned above typically has a lumen extending between its ends and an electrode extending through the lumen. In order to be able to  
10 securely connect the electrode to body tissue a helical fixation element, also called helix, is arranged at the distal end of the electrode. The helix is extendable and retractable within the lumen by means of rotating the  
15 helix. The tip of the helix is sharp in order to easily penetrate body tissue. In order to be able to provide good guidance to a user who is going to fasten the helix in the body tissue, a radiopaque ring is applied as close to the distal end of the header as possible. The ring is used as a marker, or position reference, for the position  
20 of the helix.

One example of such a lead is disclosed in US 7,092,766, Salys et al. The lead is provided with a collar, which is a radiopaque ring, at the very distal end of the lead. The collar is welded to the header,  
25 which extends proximally of the collar. It is a desire, for many reasons including avoiding shatter-noise due to electrical contact between the helix and the metal header, increasing electrode impedance, and providing good properties of interaction with the body tissue, to  
30 form the header from a polymer and having such a polymer header define the very distal end portion of the lead. Then it will not be possible to weld the header with the radiopaque ring, but it will be necessary to use an adhesive. Then a question arises regarding how to arrange

the radiopaque ring to minimize potential new problems of the adhesive fastening of the ring to the header. Also there is a general question about how to arrange the radiopaque ring at the header close enough to the distal end to maintain a good guide function.

#### SUMMARY OF THE INVENTION

It is an object of the present invention to provide a lead with a polymeric header and a radiopaque ring arranged at the header.

This object is achieved by a medical implantable lead according to the present invention as defined in claim 1.

Thus, in accordance with an aspect of the present invention, there is provided a medical implantable lead having a proximal end and a distal end, a header, which is made of a biostable and biocompatible polymer, and which is arranged at the distal end and having a first tubular portion, a helical fixation element located within the first tubular portion and being extendable from a distal end of the header, and a radiopaque ring. The header further comprises a second tubular portion, which is arranged coaxially of the first tubular portion and is attached to the first tubular portion at a distal end of the second tubular portion, while having a free proximal end, thereby forming a circumferential pocket. The first tubular portion extends from the proximal end of the header at least to said distal end of the second tubular portion, and the radiopaque ring is arranged around the first tubular portion and is received in said circumferential pocket.

Providing the header with a pocket and putting the marker ring therein is a simple solution of mounting the radiopaque ring in a shielded way, and an end portion of the helical fixation element is invisible on fluoroscopy when being inside of the ring, until it is extended from the header. Alternatively, or additionally, the radiopaque

ring is used as a position reference in cooperation with a proximal radiopaque movable part, which follows the helix when the helix is extended or retracted. Further, the radiopaque ring is mountable from the proximal end of the header by simply moving it distally along the first tubular portion and into the pocket.

For the purposes of this application, the expression that the helical fixation element is "extendable from the distal end" means that it can be moved distally out of the distal end. Typically this is obtained by rotating the helical fixation element.

In accordance with an embodiment of the medical implantable lead, it further has a ring electrode, which is arranged at the header and connected to a conductor. The conductor extends between the ring electrode and the proximal end of the lead. The ring electrode is arranged adjacent to the radiopaque ring, and has the same outer diameter as the second tubular portion. Thereby the ring electrode as well as the radiopaque ring is easily mountable onto the header.

In accordance with an embodiment of the medical implantable lead, the ring electrode and the radiopaque ring are welded together. Thereby the mounting is further facilitated and shatter-noise, due to the rings having irregular contact with each other, is avoided.

In accordance with an embodiment of the medical implantable lead, an insulating layer is applied between the radiopaque ring and the ring electrode. The same advantage as by welding is obtained in this embodiment.

In accordance with an embodiment of the medical implantable lead, the ring electrode is arranged at a distance from the radiopaque ring, and has the same outer diameter as the second tubular portion. The lead further comprises a sleeve enclosing the first tubular portion between said ring electrode and said radiopaque ring and having the same diameter as the second tubular portion.

This is an alternative way of arranging the ring electrode.

In accordance with an embodiment of the medical implantable lead, the ring electrode is radiolucent.

5 Thereby, even if the ring electrode is placed adjacent to the radiopaque ring, the radiopaque ring alone provides a distinct position of the helical fixation element.

In accordance with an embodiment of the medical implantable lead, a distal end surface of the header is  
10 textured such as to obtain an increased friction towards a biological tissue relative to a smooth surface. This embodiment is, inter alia, advantageous in that it reduces the risk of the header rotation along with the helical fixation element when it is to be extended by  
15 rotation thereof. In another embodiment of the lead according to the present invention, the texture is chosen such as to generate an enhanced response from the body tissue, which is engaged with the surface.

20 These and other aspects, features, and advantages of the invention will be apparent from and elucidated with reference to the embodiments described hereinafter.

#### BRIEF DESCRIPTION OF THE DRAWINGS

The invention will now be described in more detail  
25 and with reference to the appended drawings in which:

Fig. 1 is a schematic side view of a medical implantable lead;

Figs. 2 and 3 are cross-sectional views of  
embodiments of leads having different configurations of  
30 the elements at the distal end of the lead; and

Fig. 4 is a perspective view of a distal end portion of an embodiment of the lead.

#### DESCRIPTION OF PREFERRED EMBODIMENTS

35 Referring to Fig. 1 a medical implantable lead 1 has a proximal end 3 and a distal end 5. At the distal end 5 a helical fixation element 7 is arranged within a lumen

39, see Fig. 2, of the lead 1. The helical fixation element, which below will be referred to as a helix, 7 is extendable from the distal end 5, and retractable into the lumen. In Fig.1 it is shown in the extended position.  
5 The lead shown in Fig. 1 is most schematic but also general figure of a lead. Thus, the description thereof is valid for all embodiments that will be described below. For example the lead 1 is used with a pulse generator, where the distal end 5 thereof is introduced  
10 into a cardiac cavity.

In accordance with a first embodiment of the lead according to the present invention, as shown in Fig. 2, a distal end assembly of the lead 21 comprises a header 23, a radiopaque ring, or marker ring, 31, ring electrode 33,  
15 a helix 37, and a shaft 41. The header 23 has a proximal end 27 and a distal end 25, which constitutes the distal end of the lead 1 as well. The header 23 has a first tubular portion 24, reaching between its ends 27, 25, within which the helix 37 is arranged. The helix is  
20 attached to the shaft 41, at a distal portion thereof, and the shaft 41 is attached to an inner conductor 45, which extends through a central lumen, defined by an inner insulating tube 56, of the lead 21 to the proximal end of the lead 21. The helix 37 is electrically  
25 connected with the inner conductor 45 via the shaft 41. At a proximal end portion thereof the header 23 is attached to a tubular coupling 43, which extends proximally thereof. More particularly, in this embodiment a distal end portion 47 of the coupling 43 reaches into  
30 the header 23 and engages therewith. The connection is secured by means of a snap lock arrangement 49 consisting of a circumferential rim on the inner surface of the header 23 and a corresponding circumferential groove on the outer surface of the coupling 43, in which the rim is  
35 received. One alternative solution is to apply an adhesive instead. A portion of the shaft 41 extends within a portion of the coupling 43 and is movably supported by

the coupling 43, which can be considered as a bearing for the shaft 41.

The inner insulating tube 56 of the lead 21 extends coaxially of the inner conductor 45. At a distal end portion of the inner tube 56 it has been pushed onto and engages with a proximal end portion of the coupling 43.

It should be noted that the form and arrangement of the helix 37, the shaft 41, the inner conductor 45, and the coupling 43, as shown and described in conjunction with Fig. 2, is not central for the invention, but is a mere example of an environment in which the header 23 is used. Thus, the arrangement of the helix, the shaft, etc. can be done according to any known or future arrangement that is applicable in cooperation with the header of this invention, as defined by the appended claims.

According to the first embodiment the header 23 is further provided with a second tubular portion 29 which is arranged coaxially of the first tubular portion 24, and which is attached to the first tubular portion at a distal end 30 of the second tubular portion 29, while having a free proximal end 32, thereby forming a circumferential pocket. Thus, the second tubular portion 29 can be seen as a circular tongue protruding proximally from the attachment at the distal end 30 of the second tubular portion 24. In this embodiment the first tubular portion 24 extends from the proximal end 27 of the header 23 to the distal end 30 of the second tubular portion 29. Thus, the distal ends 25, 30 of the first and second portions 24, 29 coincide. The longitudinal length of the second tubular portion 29 is but a small fraction of the length of the first tubular portion 24. The marker ring 31 is arranged around the first tubular portion 24 and is received in the circumferential pocket. Here the marker ring 31 entirely fills the pocket. In other words the length, along the lead 21, of the marker ring 31 corresponds with the depth of the pocket, and the thickness, radially of the lead 21, of the marker ring 31

corresponds with the width of the pocket. When mounting the marker ring 31 it is slipped onto the first tubular portion 24 of the header 23 from the proximal end 25 thereof, along the first tubular portion 24 and into the pocket between the inner wall of the second tubular portion 29 and the outer wall of the first tubular portion 24.

The ring electrode 33 is arranged adjacent to the marker ring 31, and a thin insulating layer is applied between the marker ring 31 and the ring electrode 33. Alternatively, the marker ring 31 and the ring electrode 33 have been welded together before mounting on the header 23. The ring electrode 33 is electrically connected with an outer conductor 51, which extends between the ring electrode 33 and the proximal end of the lead 21. The outer conductor 51 is a coil conductor and is arranged outside and coaxially of the inner insulating tube 56. The ring electrode 33 is connected with the outer conductor 51 via a conducting strip 53, which is arranged in a groove at the outer surface of the inner tubular portion 24 of the header 23, and a ring shaped interface element 55. The interface element 55 is mounted on the coupling 43. Thus, on one hand the strip 53 is attached to the interface element 55, and on the other hand the outer conductor 51 is attached to the interface element .

An outer insulating tube 35 has been slipped over the outer conductor 51 into abutment against the distal end surface of the ring electrode. The outer diameters of the outer insulating tube 35, the ring electrode 33 and the second tubular portion 29 of the header 23 are the same, and thereby a smooth outer surface of the lead 21 has been achieved.

When the helix 37 is in the fully retracted position, the tip of the helix 37 is preferably, but not necessarily, positioned in the marker ring 31 and is thereby invisible to an operator, who uses some kind of

radioscopy to see the lead 21, and in particular the helix 37, when mounting it within a human body. When the helix 37 is extended distally, out of the header 23, typically performed by the operator rotating the inner conductor 45 at the proximal end thereof, the tip of the helix 37 becomes visible to the operator distally of the marker ring 31. As mentioned above, the marker ring 31 is alternatively, or additionally, used as a position reference for a movable radiopaque part of the lead. For instance, such a movable part is the shaft 41, and more particularly the distal end thereof, where the operator monitors the distance between that distal end and the marker ring 31.

In accordance with a second embodiment of the lead according to the present invention, as shown in Fig. 3, the ring electrode 307 has been positioned differently than in the first embodiment. As in the first embodiment, the lead 301 includes a header 303, which has first and second tubular portions 312 and 313, which form a pocket 315, wherein a marker ring 305 has been received. However, adjacent to the marker ring 305 a header sleeve 309 is arranged. The header sleeve 309 encompasses the first tubular portion 312 proximally of the marker ring 305, and protrudes a bit proximally of the header 303. The ring electrode follows proximally of the header sleeve 309, and an outer insulating tube 311 engages with the proximal end of the ring electrode 307. In this embodiment an outer coil conductor 317 has been welded directly to the ring electrode 307.

In all embodiments the header is made of a biostable and biocompatible polymer. An example of a useful, and preferred, polymeric material is PEEK, i.e. Polyetheretherketone. Other useful polymeric materials are polysulfone and PMMA (Polymethylmethacrylate). The radiopaque ring, or marker ring, is preferably made of Ta (Tantalum), while the ring electrode preferably is made of a radiolucent material, such as TiN (Titanium

Nitride), or of a TiN coated Ti substrate. An alternative to Ta for the marker ring is PtIr (Platinum Iridium) .

By making the header of a polymer, new possibilities of providing the very distal end thereof with a particular surface texture, that has advantageous additional properties compared to a general smooth surface, arise. Thus, referring to Fig. 4, which shows a header portion with the header 403, the marker ring 405, and the ring electrode 407, the end surface, or front surface, 409 of the header 403 is textured. This end surface 409 has the function of cooperating with body tissue. For example, in a pacemaker application, the end surface is engaging with cardiac tissue, where problems of for example fibrosis, inflammation, and high pace thresholds are common. Such problems are decreasable by providing the end surface 409 with an appropriate texture, which is enabled in accordance with this invention. A texture can also be applied in order to increase the friction against the tissue, thereby preventing the header 403 from being brought along in the rotation when the helix is rotated.

Above, one embodiment of the medical implantable lead according to the present invention has been described. This should be seen as merely a non-limiting example. As understood by a skilled person, many modifications and alternative embodiments are possible within the scope of the invention.

It is to be noted, that for the purposes of this application, and in particular with regard to the appended claims, the word "comprising" does not exclude other elements or steps, that the word "a" or "an", does not exclude a plurality, which per se will be apparent to a person skilled in the art.

## CLAIMS

1. A medical implantable lead having a proximal end and a distal end, a header, which is made of a biostable and biocompatible polymer, and which is arranged at the 5 distal end and having a first tubular portion, a helical fixation element located within the first tubular portion and being extendable from a distal end of the header, and a radiopaque ring, wherein the header further comprises a 10 second tubular portion, which is arranged coaxially of the first tubular portion and is attached to the first tubular portion at a distal end of the second tubular portion, while having a free proximal end, thereby forming a circumferential pocket, wherein said first 15 tubular portion extends from the proximal end of the header at least to said distal end of the second tubular portion, and wherein said radiopaque ring is arranged around the first tubular portion and is received in said circumferential pocket.

20

2. A medical implantable lead according to claim 1, further comprising a ring electrode arranged at the header and connected to a conductor, which extends between the ring electrode and the proximal end of the 25 lead, wherein the ring electrode is arranged adjacent to the radiopaque ring, and has the same outer diameter as the second tubular portion.

3. A medical implantable lead according to claim 2, 30 wherein said ring electrode and said radiopaque ring are welded together.

4. A medical implantable lead according to claim 3, wherein an insulating layer is applied between said 35 radiopaque ring and said ring electrode.

5 . A medical implantable lead according to any one of the preceding claims, further comprising an outer insulating tubing, which extends coaxially of the first tubular portion and encloses a portion thereof, which has  
5 an outer diameter that is equal to that of the second tubular portion, and which, at a distal end thereof, abut against said ring electrode.

6 . A medical implantable lead according to claim 1,  
10 further comprising a ring electrode arranged at the header and connected to a conductor, which extends between the ring electrode and the proximal end of the lead, wherein the ring electrode is arranged at a distance from said radiopaque ring, and has the same  
15 outer diameter as the second tubular portion, and wherein the medical implantable lead further comprises a sleeve enclosing said first tubular portion between said ring electrode and said radiopaque ring and having the same diameter as the second tubular portion.

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7 . A medical implantable lead according to any one of claims 2-6, wherein said ring electrode is radiolucent .

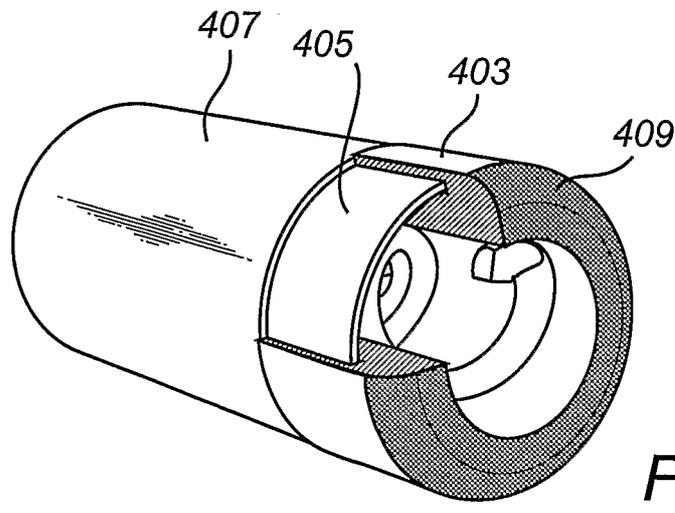
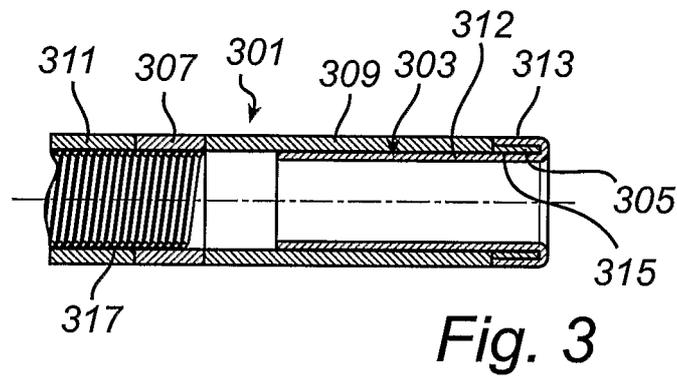
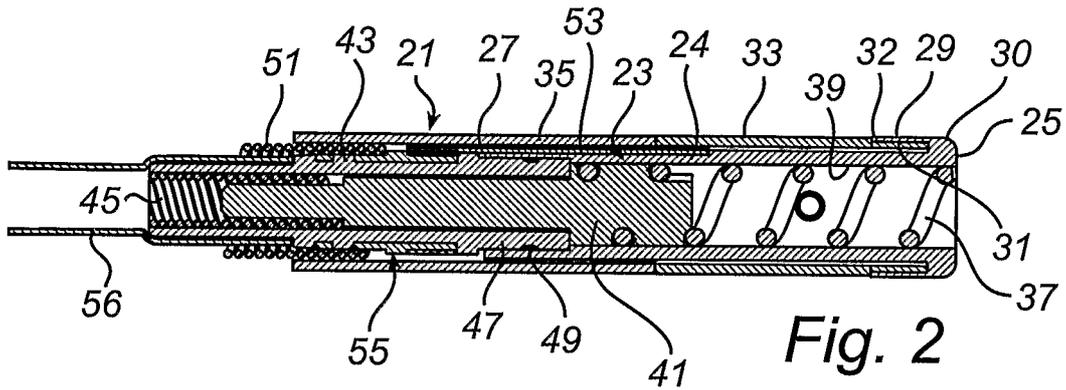
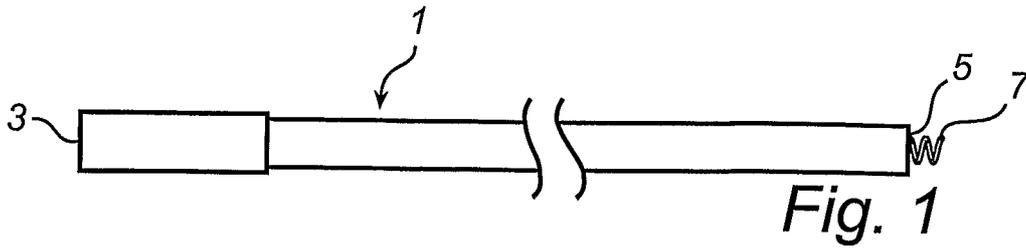
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8 . A medical implantable lead according to any one of the preceding claims, wherein a distal end surface of said header is textured such as to obtain an increased friction towards a biological tissue relative to a smooth surface .

30

9 . A medical implantable lead according to any one of the preceding claims, wherein a distal end surface of said header is textured such as to obtain an enhanced response from a biological tissue engaged with the  
35 surface.

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## INTERNATIONAL SEARCH REPORT

International application No.

PCT/SE2007/000412

## A. CLASSIFICATION OF SUBJECT MATTER

IPC: see extra sheet

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC: A61N

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

SE, DK, FI, NO classes as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-INTERNAL, WPI DATA, PAJ

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
E	WO 07123443 20 (ST. JUDE MEDICAL AB), 1 November 2007 (01.11.2007), page 8, line 27 - page 9, line 35, figure 2 --	1-9
A	US 6129751 A (LUCCHESI, A J ET AL), 10 October 2000 (10.10.2000), column 5, line 54 - line 56, figure 2 --	1-9
A	US 7092766 B1 (SALYS, S ET AL), 15 August 2006 (15.08.2006), figure 2, claim 1 --	1-9
A	US 5456708 A (DOAN, P D ET AL), 10 October 1995 (10.10.1995), column 5, line 6 - line 12, figure 1 --	1-9

 Further documents are listed in the continuation of Box C. See patent family annex.

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International application No.

PCT/SE2007/000412

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 9619259 A1 (INTERMEDIX, INC.), 27 June 1996 (27.06.1996), page 6, line 10 - line 20  --	1-9
A	EP 0795343 A2 (MEDTRONIC, INC.), 18 February 1997 (18.02.1997), figure 2  -- -----	1-9

**International patent classification (IPC)****A61N 1/05** (2006.01)**A61N 1/02** (2006.01)**Download your patent documents at [vrww.prv.se](http://vrww.prv.se)**

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Paper copies can be ordered at a cost of 50 SEK per copy from PRV InterPat (telephone number 08-782 28 85) .

Cited literature, if any, will be enclosed in paper form.

**INTERNATIONAL SEARCH REPORT**

Information on patent family members

29/12/2007

International application No.

PCT/SE2007/000412

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