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(54) **HYDROGELS A INDICE DE REFRACTION ELEVE, PREPARES
A PARTIR DE POLYMERES ET DE COPOLYMERES DE
N-BENZYL-N-METHYLACRYLAMIDE**

(54) **HIGH REFRACTIVE INDEX HYDROGELS PREPARED FROM
POLYMERS AND COPOLYMERS OF N-BENZYL-N-
METHYLACRYLAMIDE**

(57) Cette invention se rapporte à de nouveaux hydrogels biocompatibles très résistants, utiles dans des cristallins artificiels. Ces hydrogels sont optiquement transparents, ils ont des indices de réfraction élevés et ils sont stables à long terme. Ces hydrogels sont préparés à partir de copolymères réticulés de N-benzyl-N-méthylacrylamide.

(57) Novel biocompatible, high strength hydrogels useful in intraocular lenses are provided which are optically transparent, have high refractive indices and possess long term stability. The hydrogels are prepared from cross-linked copolymers of N-benzyl-N-methylacrylamide.

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(54) Title: HIGH REFRACTIVE INDEX HYDROGELS PREPARED FROM POLYMERS AND COPOLYMERS OF N-BENZYL-N-METHYLACRYLAMIDE (57) Abstract Novel biocompatible, high strength hydrogels useful in intraocular lenses are provided which are optically transparent, have high refractive indices and possess long term stability. The hydrogels are prepared from cross-linked copolymers of N-benzyl-N-methylacrylamide.		

**HIGH REFRACTIVE INDEX HYDROGELS PREPARED
FROM POLYMERS AND COPOLYMERS OF
N-BENZYL-N-METHYLACRYLAMIDE**

BACKGROUND OF THE INVENTION

Field of the Invention

The present invention relates to hydrogels. More particularly, this invention relates to optically transparent, high refractive index, high strength hydrogels which are especially useful in the fabrication of intraocular lenses. In one of its more particular aspects, this invention relates to a novel monomer for use in producing such hydrogels. In another of its more particular aspects, the present invention relates to intraocular lenses prepared from such hydrogels.

Description of Related Art

10 Since the early 1940s, optical devices in the form of intraocular lenses have been utilized to replace the natural physiological crystalline ocular lens in humans and other mammals. Typically, the intraocular lens is implanted within the ocular environment immediately after surgically removing the natural lens which has become opaque or otherwise damaged by cataract formation or injury.

15 For decades the most prevalently utilized materials for forming intraocular lenses were acrylates or methacrylates and particularly polymethylmethacrylate, a rigid, glassy polymer. However, since full-size polymethylmethacrylate intraocular lenses have diameters in the range of 8-13 mm, relatively large incisions were necessary in order to remove the natural lens and insert the intraocular lens.

20 Recently developed surgical techniques and improved instrumentation have made it possible to remove the opaque or damaged natural lens through incision sizes as small as 2 - 3 mm. Because small incision surgery is much less traumatic for patients and decreases complications and healing time, this technique has become the method of choice for a large number of ophthalmic surgeons.

25 A number of different intraocular lens designs and materials have been developed for use in connection with small incision surgical techniques. One approach utilizes the concept of preparing lenses from elastomeric materials such

as silicones and thermoplastic polymers. Prior to surgically inserting the elastomeric lens, the surgeon rolls or folds the lens so that it is reduced in size for passing into the eye through a smaller incision. Once placed within the eye, the lens unfolds or unrolls to its full size.

5 One problem associated with these elastomeric lenses is the possibility that permanent deformation or crease marks may occur when the lens is folded or rolled. This is especially a concern at the center of the lens optical zone where most of the rolling or folding deformation takes place.

Another approach to providing a small incision intraocular lens is suggested
10 in U.S. Patent No. 4,731,079. This reference discloses an intraocular lens formed of a polymer having a softening or glass transition temperature less than 42°C and preferably about body temperature. The lens can be heated to above its softening temperature and deformed by compression or elongation to reduce at least one dimension. Then, by cooling the lens at a temperature substantially below its
15 softening temperature, the lens will remain in the deformed configuration until it is warmed. Ophthalmic surgeons can implant the deformed lens and once the lens warms to body temperature it returns to its original configuration.

A major problem associated with these intraocular lenses is the limited number of polymers available for preparing the lenses. Polymethylmethacrylate has a glass
20 transition temperature of 100°C and thus cannot be used to form these lenses. Most acrylates and methacrylates have similarly high glass transition temperatures. Though formulating the lenses with plasticizers will lower the glass transition temperature, the presence of plasticizers in intraocular lenses is generally unacceptable to most surgeons because of potential leaching problems. Alterna-
25 tively, water is a suitable plasticizer. However, only small amounts of water, typically less than 10%, can be utilized in the polymers to place the glass transition in the appropriate range. Thus, typical hydrogels which have much higher amounts of water are not suitable for fabricating the deformable lenses.

An additional drawback with this suggested small incision intraocular lens is
30 the added degree of surgical complexity required to deform the lens into its small incision configuration. The lenses disclosed in U.S. Patent No. 4,731,079, described above, are packaged in a form that requires the implanting surgeon to

warm, deform, and cool the lens immediately prior to its implantation. This procedure is considerably more involved than traditional lens implantation techniques.

Another suggested approach for small incision lens implantation involves
5 implanting hydrogel intraocular lenses in their smaller dehydrated state. Once the
implanted dehydrated lens is secured within the eye it reportedly hydrates and swells
in the aqueous ocular environment. A significant problem associated with this
approach is the large amount of swelling required to produce an effective lens
diameter. In order to fully swell the lens from a diameter of about 3 mm to about
10 6 mm the lens must swell 8 times by volume. This translates to a lens which is
about 85% water. For larger full-size intraocular lenses the swell volume is much
higher. Since most hydrogels are structurally very weak at these high water
contents, many surgeons are reluctant to implant them. Also, these high water
content hydrogels have a very low refractive index of around 1.36. In order to
15 achieve suitable refractive powers, the hydrogel lens must therefore be thicker in the
optic portion. As a result, a dehydrated hydrogel intraocular lens that will fit
through a desirably small incision will not swell to a sufficiently large hydrated size
to effectively function as an intraocular lens. This problem is compounded if larger,
full size intraocular lenses that have optic diameters greater than 6 mm are desired.
20 In order to produce a hydrated lens having a sufficient optic diameter the dehydrated
hydrogel lens must be larger than desirable for a small incision implantation
procedure.

Alternatively, U.S. Patent No. 4,919,662 suggests rolling or folding hydrogel
intraocular lenses in their elastic hydrated form, and then dehydrating the lenses at
25 lower temperatures to fix the rolled or folded lens configuration at a size suitable
for small incision implantation. Once implanted, these lenses hydrate and swell to
the original lens configuration. This method has the disadvantage of requiring the
handling of fully hydrated lenses during the deforming process. Unfortunately,
hydrated lenses have relatively weak tensile strengths and tear strengths and
30 handling the lenses causes frequent tearing damage.

U.S. Patent No. 4,813,954 discloses expansile hydrogel intraocular lenses
which are formed by simultaneously deforming and dehydrating hydrogel intraocular

lenses prior to implanting the lenses in their dehydrated state. Lenses subjected to this treatment swell to about 180% of their reduced size. For example, lenses deformed or compressed to a diameter of 3.2 mm will swell to only about 5.8 mm. Thus, while providing some advantages over simply implanting dehydrated lenses,
5 the method and lenses described in U.S. Patent No. 4,813,954 do not result in full-size implanted intraocular lenses of over 8 mm.

In addition to size considerations, however, the constitution of the hydrogels must also be considered. The provision of high water content, optically transparent, high refractive index hydrogels which possess long term stability depends to a large
10 extent upon the make-up of the hydrogel. Since most hydrogels are composed of cross-linked copolymers, the selection of appropriate comonomers and cross-linking agents is an important consideration.

It is therefore an object of the present invention to provide cross-linked hydrogels having the properties of high water content, high refractive index, optical trans-
15 parency, high strength, and long term stability, which hydrogels are biocompatible and suitable for use as intraocular lenses. Another object of this invention is to provide methods for the preparation of such hydrogels.

Other objects and advantages of the present invention will become apparent from the following disclosure and description.

20 SUMMARY OF THE INVENTION

The present invention accomplishes the above-mentioned objectives by providing a novel series of copolymers in which one of the comonomers is N-benzyl-N-methylacrylamide (BMA), a previously unknown compound. The other comonomer or comonomers may either be derivatives of acrylic acid, such as acrylates,
25 methacrylates, acrylamides or methacrylamides; vinyl-substituted amides; or nitrogen-containing heterocyclic compounds which are substituted with unsaturated sidechains, such as vinyl or acryloyl sidechains.

The copolymers of the present invention upon cross-linking and hydration form optically transparent biocompatible hydrogels which have refractive indices in
30 the dry state of 1.53 to 1.55 and in the fully hydrated state of 1.42 to 1.49. They hydrate to an equilibrium water content in the range of 20% to 65% and are stable

for extended periods of time. The resulting hydrogels are stronger than previously available hydrogels and are useful in intraocular lenses and related applications.

Further objects, features and advantages of the present invention, as well as a better understanding thereof, will be afforded to those skilled in the art from a
5 consideration of the following detailed explanation of exemplary embodiments thereof.

DETAILED DESCRIPTION OF THE EXEMPLARY EMBODIMENTS

The present invention provides hydrophilic polymeric materials which form hydrogels. Because of their importance in the field of biomaterials and agriculture,
10 hydrogels and processes for their formation are well documented in the literature.

A preferred class of hydrogel-forming polymers includes cross-linked polymers and copolymers which hydrate to a relatively high hydrated equilibrium water content. As pointed out above, however, high water content hydrogels generally have very low refractive indices. It is, therefore, unexpected to find that
15 cross-linked copolymers of N-benzyl-N-methylacrylamide have equilibrium water contents of 20% to 65% and refractive indices ranging from 1.53 to 1.55 in the dry state and from 1.42 to 1.49 in the fully hydrated state. By using the hydrogels of this invention it is possible to provide higher refractive power in a lens or other article with a much thinner optic portion than by using the low refractive index,
20 high water content hydrogels previously available. It will be appreciated by those skilled in the art that the hydrogels of the present invention can be tailored to provide a wide range of refractive indices and hydrated equilibrium water contents, in order to accommodate a variety of utilities.

N-benzyl-N-methylacrylamide (BMA) is a novel compound. It can be
25 synthesized from N-benzylmethylaniline by reaction with acryloyl chloride. N-benzyl-N-methylacrylamide is polymerizable to form a homopolymer which has a water content less than 5% and a refractive index of 1.585. Because of these properties, homopolymers of BMA can be used in hard intraocular lenses and related applications. BMA can also be copolymerized with a wide variety of
30 comonomers to form copolymers which, upon cross-linking and hydration, yield

high water content, high refractive index hydrogels having outstanding strength characteristics.

Comonomers which can be used include:

5	alkyl acrylates (alkyl = 1-6 carbon)	3-(N,N-dimethylamino)propylacrylamide
	phenyl acrylate	allylacrylamide
	hydroxyethyl acrylate	hydroxymethyldiacetoneacrylamide
	hydroxypropyl acrylate	N,N-dimethylacrylamide
	hydroxybutyl acrylate	N,N-diethylacrylamide
10	glycerol monoacrylate	N-ethyl-N-methylacrylamide
	2-phenoxyethyl acrylate	N-methylmethacrylamide
	2-N-morpholinoethyl acrylate	N-methylolmethacrylamide
	2-(2-ethoxyethoxy)ethyl acrylate	N-(2-hydroxypropyl)methacrylamide
	2-(N,N-dimethylamino)ethyl acrylate	N-4-(hydroxyphenyl)methacrylamide
15	3-(N,N-dimethylamino)propyl acrylate	N-(3-picoly)l)methacrylamide
	alkyl methacrylates (alkyl = 1-6 carbon)	3-vinylpyridine
	furfuryl methacrylate	4-vinylpyridine
	hydroxyethyl methacrylate	N-vinylpyrrolidinone
	hydroxypropyl methacrylate	vinyl pyrazine
20	hydroxybutyl methacrylate	2-methyl-5-vinylpyrazine
	glycerol monomethacrylate	4-vinylpyrimidine
	2-phenoxyethyl methacrylate	vinyl pyridazine
	2-N-morpholinoethyl methacrylate	N-vinylimidazole
	2-(N,N-dimethylamino)ethyl methacrylate	N-vinylcarbazole
25	3-(N,N-dimethylamino)propyl methacrylate	N-vinylsuccinimide
	2-pyrrolidinonyl ethyl methacrylate	4-methyl-5-vinylthiazole
	N-alkyl acrylamides (alkyl = 1-8 carbon)	N-acryloylmorpholine
	N-(n-octadecylacrylamide)	N-methyl-N-vinylacetamide

Cross-linking agents which can be used to produce the hydrogels of the present invention include 1,3-propanediol diacrylate, 1,4-butanediol diacrylate, 1,6-hexamethylene diacrylate, 1,4-phenylene diacrylate, glycerol tris (acryloxypropyl) ether, ethylene glycol dimethacrylate, 1,3-propanediol dimethacrylate, 1,6-hexamethylene dimethacrylate, 1,10-decanediol dimethacrylate, 1,12-dodecanediol dimethacrylate, triethylene glycol dimethacrylate, glycerol trimethacrylate, N,N'-octamethylenebisacrylamide, N,N'-dodecanomethylenebisacrylamide, N,N'-(1,2-dihydroxyethylene)bisacrylamide, allyl methacrylamide, divinylpyridine, 4,6-divinylpyrimidine, 2,5-divinylpyrazine, 1,4-divinylimidazole, 1,5-divinylimidazole, and divinylbenzene.

In general, BMA is present in an amount of about 5 weight percent to 85 weight percent based on the total weight of monomers. The cross-linking agent may be used in an amount of about 0.01 weight percent to 0.50 weight percent.

The hydrogels of the present invention may also include from about 0.1 weight percent to about 10 weight percent ultraviolet (UV) radiation absorbing compounds. A large variety of hydroxybenzophenones and hydroxyphenylbenzotriazoles are commercially available and may be used for this purpose. Preferably, the UV-
5 absorbing compound is copolymerizable with the monomer forming the hydrogel polymer, thus becoming part of the final polymer or copolymer. This feature assures that the hydrated hydrogel is optically clear, and assures that the UV-absorbing compound does not leach or migrate from the article fabricated from the hydrogel, for example, from an implanted lens. An exemplary UV-absorber of this
10 type is 2-(2'-hydroxy-5'-methacryloxyethylphenyl)-2H-benzotriazole. In addition, the allyloxypropyl modified hydroxyphenylbenzotriazole, 2-[5-chloro-2H-benzotriazol-2-yl]-6-[1,1-dimethylethyl]-4-[2-propenyloxypropyl] phenol, known as Tinuvin 326, is particularly suitable because of its high absorptivity at wavelengths up to 405 nm, its solubility, and its vinyl functionality.

15 The relative amounts of the various comonomers and other reagents used to produce the hydrogel-forming materials will depend upon the desired strength, final water content, and refractive index, as well as the amount of material elasticity required to deform a lens fabricated of the hydrogel or to otherwise apply the hydrogel to a specific application. The hydrogel materials also should have
20 sufficient resiliency at their deformation temperatures to prevent permanent stretching or cracking during or after any deforming process.

Hydrogels prepared using BMA have the properties desired for use in a wide variety of applications, especially those applications requiring high strength, high hydrophilicity and long term stability. For example, the hydrogels thus prepared
25 can be used to produce polyelectrolyte gels, high water content superabsorbents, contact lenses, cornea on-lays, cornea in-lays, and other medical devices requiring these properties, as well as intraocular lenses.

The following examples are offered as being illustrative of the principles of the present invention and not by way of limitation.

Example 1

Synthesis of N-benzyl-N-methylacrylamide

A quantity of 121 g of N-benzylmethylamine was reacted with 100 g of acryloyl chloride in the presence of 111 g of triethylamine in ether at 0°C to 25°C
5 for 16 hours. The product was filtered, the solvent was removed, and N-benzyl-N-methylacrylamide was isolated in 69% yield by distillation under vacuum (bp 83°-85°C/0.04 mm - Hg).

The following example illustrates the polymerization of N-benzyl-N-methylacrylamide and various other monomers.

10

Example 2

Eleven different homopolymers and copolymers were prepared and evaluated for use as exemplary hydrogel-forming materials. Table I illustrates the proportions of each component of the polymerization mixture and the properties of the polymers obtained. Each polymerization procedure was carried out by first mixing the appropriate amounts of the monomers and cross-linker, if any, with 2,2'-azobisisobutyronitrile as a polymerization initiator. Then each mixture was transferred to an ampoule which was pretreated with a silicone grease mold releasing agent. Each ampoule and mixture was then attached to a vacuum system and cooled with liquid nitrogen. After the mixture was frozen by the liquid nitrogen, the mixture was
15 evacuated by turning on the vacuum system. Once a constant pressure was achieved, the vacuum system was turned off and the mixture was allowed to thaw by warming the ampoule in a water bath. This freeze-thaw cycle was repeated three times in order to provide sufficient mixture degassing. Finally, each mixture and ampoule were sealed under vacuum or an inert gas such as nitrogen or argon and
20 polymerized at a temperature of 60°C for a period of 36 hours, then at 135°C for
25 12 hours.

After the polymerized material was cooled, the ampoule was broken open and the resulting polymer rod was cut into blanks. Each blank was then machined to an expansile intraocular lens in its dehydrated state. The machined dehydrated

lenses have diameters ranging from approximately 4.5 to 7.1 mm and cross-sectional thicknesses ranging from approximately 2.3 to 3.6 mm.

Exemplary lenses were deformed by heating a water bath to 60°C and placing a beaker of heptane in the water bath. The lenses were immersed in the warm
5 heptane for approximately 10 seconds and simultaneously folded with a pair of tweezers. The folded lenses were then removed from the heptane and inserted into 1/16 inch I.D. silicone tubes. The tubes and folded lenses were then immersed in the warm heptane for 10 - 20 seconds. The tubes and lenses were removed from the heptane and immediately rolled and squeezed between two fingers, compressing
10 the lenses into tightly folded and elongated shapes. The elongated lenses and tubes were allowed to cool to room temperature and then the lenses were removed from the tubes. At room temperature the lenses remained in their elongated state. The long dimension ranges from approximately 8 to 13 mm, the cross-sectional width ranges from approximately 2 to 4 mm, and the cross-sectional height ranges from
15 approximately 1.8 to 3.0 mm.

Each lens was immersed in physiologically buffered aqueous solutions for 8-48 hours and allowed to hydrate to its equilibrium water content. The lenses were observed to expand and re-form to the original configuration. The enlarged reconfigured hydrated lenses have expanded diameters ranging from approximately
20 8.5 to 9.5 mm and expanded cross-sectional thicknesses of approximately 4.5 mm.

The abbreviations utilized in Table I are identified immediately following the table.

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TABLE I.

Experi- ment No.	Weight Percent										n _D ³⁷		Strength		Elon- gation %	Duro- meter Shore A	H ₂ O %
	BMA	DMA	NVP	HEMA	PEMA	DEA	BEA	EGDMA	UV- ABSORBER	Dry	Wet	Tensile (psi)	Tear (pli)				
1		100								1.51	1.34					>98	
2	5	45		50				0.01		1.52	1.39					65	
3	33.4	65.2						0.34	1	1.535	1.42	18	2	330		57	
4				100						1.51	1.44					39	
5	30	35		35				0.02	2	1.535	1.46	75	9	440	12	36	
6	22	10		68				0.17	2	1.532	1.482	180	45	150	27	24	
7	25	5		70				0.4	2	1.535	1.49	320	83	230	31	22	
8	100									1.585	1.58					< 5	
9	85	15															
10	60	40															
11	10	50		40													
12	34	19	20	27				0.15	1.2	1.542						34	
13	38	31		24	7			0.04	1.2	1.542						30	
14	40					60		0.01	1.4								
15						69	31	0.01	1.4								
16	43	49				8		0.01	1.2	1.547						38	
17	38	45				17		0.01	1.2	1.541						43	

BEA N-benzyl-N-ethylacrylamide DMA N,N-dimethylacrylamide UV-ABSORBER 2-(2'-hydroxy-5'-methacryloyloxyethylphenyl)-2H-benzotriazole
 BMA N-benzyl-N-methylacrylamide EGDMA ethylene glycol dimethacrylate NVP N-vinylpyrrolidinone
 DEA N,N-diethylacrylamide HEMA 2-hydroxyethyl methacrylate PEMA 2-pyrrolidinonyl ethyl methacrylate

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Because of the outstanding properties of hydrogels produced using the novel monomers of the present invention including their optical transparency, their high water content, and their high refractive index, they display extremely good optical resolution efficiency.

5 Thus, the use of the novel monomers of the present invention results in hydrogels which display excellent optical properties, as well as excellent stability.

10 Having thus described exemplary embodiments of the present invention, it should be noted by those skilled in the art that the disclosures herein are exemplary only and that alternatives, adaptations, and modifications may be made within the scope of the present invention.

WHAT IS CLAIMED IS:

1. N-benzyl-N-methylacrylamide.
2. A homopolymer comprising polymerized N-benzyl-N-methylacrylamide.
3. A hydrogel comprising a cross-linked copolymer prepared from a mixture of comonomers comprising N-benzyl-N-methylacrylamide and at least one comonomer polymerizable with said N-benzyl-N-methylacrylamide.
4. The hydrogel of claim 3 wherein said at least one comonomer polymerizable with said N-benzyl-N-methylacrylamide is selected from the group consisting of acrylates, methacrylates, acrylamides, methacrylamides, vinyl-substituted amides, vinyl-substituted nitrogen-containing heterocyclic compounds,
5 and acryloyl-substituted nitrogen-containing heterocyclic compounds.
5. The hydrogel of claim 3 wherein said at least one comonomer polymerizable with said N-benzyl-N-methylacrylamide is selected from the group consisting of methyl acrylate, ethyl acrylate, propyl acrylate, butyl acrylate, amyl acrylate, hexyl acrylate, phenyl acrylate, hydroxyethyl acrylate, hydroxypropyl
5 acrylate, hydroxybutyl acrylate, glycerol monoacrylate, 2-phenoxyethyl acrylate, 2-N-morpholinoethyl acrylate, 2-(2-ethoxyethoxy)ethyl acrylate, 2-(N,N-dimethyl-amino)ethyl acrylate, 3-(N,N-dimethylamino)propyl acrylate, methyl methacrylate, ethyl methacrylate, propyl methacrylate, butyl methacrylate, amyl methacrylate, hexyl methacrylate, furfuryl methacrylate, hydroxyethyl methacrylate, hydroxy-
10 propyl methacrylate, hydroxybutyl methacrylate, glycerol monomethacrylate, 2-phenoxyethyl methacrylate, 2-N-morpholinoethyl methacrylate, 2-(N,N-dimethyl-amino)ethyl methacrylate, 3-(N,N-dimethylamino)propyl methacrylate, 2-pyrrolidinonyl ethyl methacrylate, N-methylacrylamide, N-ethylacrylamide, N-propylacrylamide, N-butylacrylamide, N-amylacrylamide, N-hexylacrylamide, N-heptylacrylamide, N-octylacrylamide, N-(n-octadecylacrylamide), 3-(N,N-dimethyl-
15 amino)propylacrylamide, allylacrylamide, hydroxymethyl diacetoneacrylamide,

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N,N-dimethylacrylamide, N,N-diethylacrylamide, N-ethyl-N-methylacrylamide, N-methylmethacrylamide, N-methylolmethacrylamide, N-(2-hydroxypropyl)methacrylamide, N-4-(hydroxyphenyl)methacrylamide, N-(3-picolyl)methacrylamide, 20 3-vinylpyridine, 4-vinylpyridine, N-vinylpyrrolidinone, vinyl pyrazine, 2-methyl-5-vinylpyrazine, 4-vinylpyrimidine, vinyl pyridazine, N-vinylimidazole, N-vinylcarbazole, N-vinylsuccinimide, 4-methyl-5-vinylthiazole, N-acryloylmorpholine, and N-methyl-N-vinylacetamide.

6. The hydrogel of claim 3 wherein said at least one comonomer polymerizable with said N-benzyl-N-methylacrylamide is selected from the group consisting of N,N-dimethylacrylamide, N,N-diethylacrylamide, 2-hydroxyethyl methacrylate, N-vinylpyrrolidinone, and 2-pyrrolidinonyl ethyl methacrylate.

7. The hydrogel of any of claims 3 to 6 wherein said mixture of comonomers includes a cross-linking agent selected from the group consisting of 1,3-propanediol diacrylate, 1,4-butanediol diacrylate, 1,6-hexamethylene diacrylate, 1,4-phenylene diacrylate, glycerol tris (acryloxypropyl) ether, ethylene glycol 5 dimethacrylate, 1,3-propanediol dimethacrylate, 1,6-hexamethylene dimethacrylate, 1,10-decanediol dimethacrylate, 1,12-dodecanediol dimethacrylate, triethylene glycol dimethacrylate, glycerol trimethacrylate, N,N'-octamethylenebisacrylamide, N,N'-dodecanomethylenebisacrylamide, N,N'-(1,2-dihydroxyethylene)bisacrylamide, allyl methacrylamide, divinylpyridine, 4,6-divinylpyrimidine, 2,5-divinylpyrazine, 10 1,4-divinylimidazole, 1,5-divinylimidazole, and divinylbenzene.

8. An intraocular lens fabricated from the homopolymer of claim 2.

9. An intraocular lens fabricated from the hydrogel of any of claims 3 to 6.

10. The hydrogel of any of claims 3 to 6 having a refractive index, n_D^{37} , of 1.53 to 1.55 in the dry state and 1.42 to 1.49 in the fully hydrated state.

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11. The hydrogel of any of claims 3 to 6 having an equilibrium water content of 20% to 65%.

12. A process for preparing N-benzyl-N-methylacrylamide which comprises reacting N-benzylmethylamine with acryloyl chloride.