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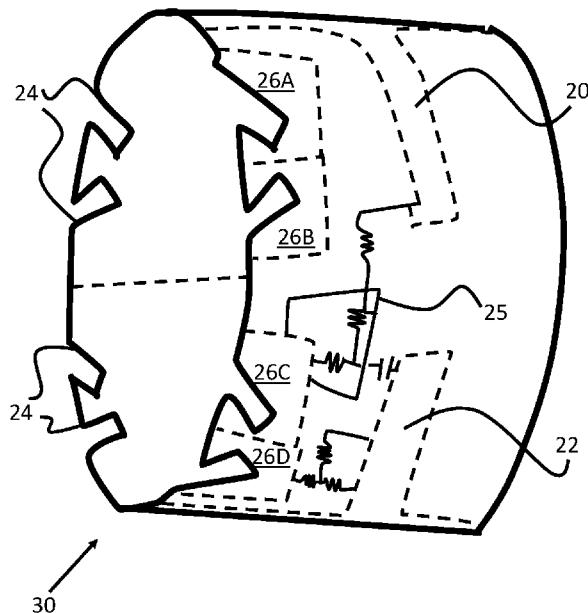


Figure 6

(57) Abstract: A circuit system includes a user interface, voltage source, and a terminal bank connected to the voltage source. The circuit can be used in a powered catheter system where the catheter includes a structural reinforcement layer such as a braid comprised of one or more wires. The reinforcement layer can be used to convey a current or signal in a powered catheter. The catheter may utilize a hypotube element which provides integrated sensors in order to power and control multiple systems in the powered catheter.

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[0007] In another embodiment a circuit system utilizes a voltage source, a terminal bank, and one or more sensors which connect to the terminal bank.

[0008] In another embodiment a circuit system utilizes a hypotube, where the hypotube includes a terminal bank and one or more sensors.

[0009] In another embodiment a braided catheter utilizes some of the wires comprising the braid to convey current in a circuit.

[0010] In another embodiment a braided catheter utilizes some of the wires comprising the braid to convey signals in a circuit.

[0011] In another embodiment a braided catheter utilizes some of the constituent wires comprising the braid to convey current to a terminal bank.

[0012] In another embodiment a braided catheter utilizes some of the constituent wires comprising the braid to convey current to a terminal bank, where one or more sensors are connected to the terminal bank.

[0013] In another embodiment, a braided catheter comprises multiple wires where some of the constituent wires comprising the braid are used to link to a terminal bank.

[0014] In another embodiment, a braided catheter comprises multiple wires where some of the wires are used as a supply and return path for a circuit and some of the wires convey a signal.

[0015] In another embodiment, a braided catheter comprises multiple wires where some of the wires are used as a supply and return path for a circuit and some of the wires convey a signal between one or more sensors and a user interface.

[0016] In another embodiment, a braided catheter comprises a hypotube.

[0017] In another embodiment, a braided catheter comprises a hypotube, where the hypotube contains a terminal bank.

[0018] In another embodiment, a braided catheter comprises a hypotube, where the hypotube contains a terminal bank and one or more sensors.

[0019] In another embodiment a powered catheter includes a hypotube.

[0020] In another embodiment a circuit includes a hypotube, where the hypotube contains a terminal bank and one or more sensors.

[0021] In another embodiment a powered catheter includes a hypotube, where the hypotube contains a terminal bank and one or more sensors.

[0022] In another embodiment a powered catheter includes a variable coil detachment system.

[0023] In another embodiment a powered catheter includes a catheter distal tip detachment system.

[0024] In another embodiment a powered catheter includes a steerable guidewire system.

BRIEF DESCRIPTION OF THE DRAWINGS

[0025] These and other aspects, features and advantages of which embodiments of the invention are capable of will be apparent and elucidated from the following description of embodiments of the present invention, reference being made to the accompanying drawings, in which:

[0026] Figure 1 illustrates a catheter and catheter interface according to the present invention.

[0027] Figure 2 illustrates a cutaway view of an elongated tube of a catheter having a plurality of braided structural wires that are configured to delivery electrical signals between a distal end of the catheter, according to the present invention.

[0028] Figures 3A and 3B illustrate example cross sections of structural wires that delivery electrical signals according to the present invention.

[0029] Figure 4 illustrates a plan view of an interface powering several sensors located at a distal end of the catheter.

[0030] Figure 5 illustrates an interface powering several sensors via only two power wires and transmitting data signals via a plurality of data wires.

[0031] Figure 6 illustrates an example of a hypotube having a plurality of sensors, connection points and circuit paths.

[0032] Figures 7 and 8 illustrate an alternate embodiment of a hypotube having a plurality of electrical contacts arranged to contact portions of a pusher or implant located within the passage of the catheter.

[0033] Figures 9A and 9B illustrate a catheter having a hypotube with electrical contacts connected to a plurality of structural wires that supply power and that are configured to contact portions of an implant.

[0034] Figures 10 and 11 illustrate an embolic coil having a detachment location.

[0035] Figures 12 and 13 illustrate a catheter with a hypotube connected to a plurality of structural wires that supply power so as to allow selective detachment of a distal portion of a catheter.

[0036] Figure 14 illustrates a hypotube having a plurality of heater coils.

[0037] Figure 15 illustrates a hypotube having a plurality of heater coils.

DESCRIPTION OF EMBODIMENTS

[0038] Specific embodiments of the invention will now be described with reference to the accompanying drawings. This invention may, however, be embodied in many different forms and should not be construed as limited to the embodiments set forth herein; rather, these embodiments are provided so that this disclosure will be thorough and complete, and will fully convey the scope of the invention to those skilled in the art. The terminology used in the detailed description of the embodiments illustrated in the accompanying drawings is not intended to be limiting of the invention. In the drawings, like numbers refer to like elements.

[0039] It should be understood that a variety of different embodiment and/or variations on components are described herein. It is the intention of this application that each of

these embodiments and components can be used and/or interchanged with each other. Therefore, while a specific embodiment may not specify a feature of another embodiment described herein, such a combination is contemplated and included in the present invention.

[0040] Figure 1 illustrates a catheter 10 (or alternately a microcatheter) that delivers power and data through structural wires that make up the elongated tubular portion 11 of the catheter 10. The catheter 10 is connected to an interface 16 that provides power and/or data to and from the catheter via a cable 15. By allowing the structural wires to be used for power/data, the catheter size or diameter can be minimized. Additionally, a plurality of electrically powered components (e.g., sensors) and even circuitry can be used in the distal end 11A (or other locations) in the catheter 10.

[0041] While some of the embodiments of the present invention may be described in terms of powering and obtaining data from electrical components such as sensors, it should be understood that a variety of different powered elements are possible. For example, heater coils, mechanical latches, and similar powered implant detachment mechanisms can be powered according to the present invention. In other examples, other powered elements may include imaging systems, pressure sensing, temperature sensing, and oxygen sensing.

[0042] Figure 2 illustrates a plurality of braided structural wires 18 that are part of the elongated tubular portion 11 of the catheter 10 that terminate with and connect to a distally located receptacle 12. These wires 18 provide structural support to the elongated tubular portion 11 and also can be used to deliver electrical power and/or data to the proximal end of the catheter 10. The braid of Figure 1 is comprised of 8 wires (18A-18F) braided in a tubular shape. The braided wires 18 can be located in several different positions as part of the elongated tubular portion 11, such as 1) on an outer surface of the tubing of the elongated tubular portion 11, 2) “sandwiched” between two or more layers of the tubular portion 11 (i.e., not exposed on an interior or exterior of the tubing), and 3) located along the inner surface of the tubular portion 11 so as to be exposed to the interior passage of the tubular portion 11.

[0043] In one embodiment shown in Figure 3A, the braided structural wires 18 may be a metal material 25 that is structurally suitable for a catheter (e.g., nitinol or stainless steel) and are coated with a highly conductive layer 23 (e.g., gold) and then coated in an electrical insulation 21 (e.g., polyamide).

[0044] In another embodiment shown in Figure 3B, the braided structural wires 18 comprising the tubular braid are made entirely of a conductive material 23 (e.g., gold) in order to efficiently convey the current/signal, and further includes an electrically insulating coating 23 preventing discharge of the current/signal while it is being conveyed. While the wires 18 are depicted as having a round or circular cross section in Figures 3A and 3B, other shapes are also possible, such as relatively flat, oval, rectangular, and square.

[0045] Figure 4 illustrates an abstract schematic diagram of an example circuit system having four electrical components (26A-26D) and a plurality of structural wires 18. Each electrical components 26A-26D is connected to two wires that are connected to a positive and negative terminal of a power source in the interface 16, which thereby supplies power to the electrical components. In this respect, the 8 wire example shown in Figure 2 can be used to power all of the electrical components and to communicate data back to the interface 16. Similarly, a 10 wire braid would allow 5 electrical components, and a 16 wire braid would allow 8 electrical components since each electrical components would require 2 wires 18 to complete the circuit. In this respect, any number of wires can be used, such as 2, 4, 6, 8, 10, 12, 14, 16, and 18.

[0046] Figure 5 illustrates another embodiment of a circuit configuration in which only two of the wires 18 provide power via a positive and negative voltage source (e.g., battery) of the interface 16. The wires connect to separated electrical terminals 20 and 22 which are located at or near the distal end 11A of the catheter 10. The electrical components 26A-26D are each connected to these terminals 20, 22 via wires 17 (or any other electrical path), allowing power to be supplied from the interface 16 to each of the electrical components.

[0047] The data or signal from each of the electrical components 26A-26D is then conveyed from the electrical components to the user interface via one of the braided wires 18 of the catheter 10. In this way, for example, an 8-wire braid can utilize up to 6 electrical

components instead of 4 electrical components. Similarly, a 10-wire braid could utilize up to 8 electrical components (two wires used for the positive and negative terminal connection, and the balance of the wires used to connect each electrical components), a 12-wire braid could utilize up to 10 electrical components, and so on.

[0048] It should be understood that some electrical components (such as sensors) require only two power wires to operate and send back data (e.g., such as a thermistor in which changes in resistance on the wires is measured), while other electrical components or sensors require one or more additional wires to convey data (e.g., three wires total). As such, the number of wires used in each of these embodiments also depends on the type of electrical components used.

[0049] The user interface 16 preferably acts as a point of control for the user (e.g., press a button 16A) to effect an outcome at the other end of the system (e.g., detach an implant or a distal portion 11A of the catheter 10). Where the electrical components are used for sensing the physiological conditions of the vessel (e.g., pressure or temperature), the user interface may have a display 16B (as well as the underlying CPU/microprocessor, memory, and software to process data and drive the display) indicating the particular physiological condition which is observed. The user interface 16 also preferably contains the voltage source for the circuit, in one example via a battery with a positive and negative terminal.

[0050] In one embodiment, the terminal banks and electrical components configuration of Figure 5 can be formed by a hypotube located near the distal end of a catheter 10, similar to receptacle 12 of Figure 2. This can be visualized by taking the circuit concept of the distal part of the circuit of Figure 5 (i.e. the left side of the figure, comprising the terminal banks 20, 22 and electrical components 26A-26D) and configuring it into a cylindrical or circle shape. Figure 6 illustrates a hypotube representation 30 of such a circuit. The hypotube 30 contains a plurality of notched or cut-out areas 24 which the distal end of the braid wires 18 connect to and/or otherwise mate within. The wires 18 of the braid can be welded or otherwise electro-mechanically joined to the cut-out sections 24 to create a snug connection with the hypotube 30.

[0051] The hypotube 30 may also contain embedded circuitry 25. This circuitry 25 may connect to the electrical components 26A-26D, so as to provide additional functionality and/or processing of electrical components signals. This circuitry 25 may also be connected to the positive and negative voltage terminal banks 20, 22, as indicated by element 26 in Figure 5, so as to obtain power for the circuitry 25.

[0052] The hypotube 30 may be cut (e.g., laser cut) into a pattern to include the cut-out sections 24. The hypotube 30 is preferably made of materials which are highly conductive, have high mechanical strength, and allow for easy termination/connectivity of other wires and materials. In one example, the hypotube is comprised of a gold plated polyimide and additional laser cuts can be performed to help shape the path of the different electrical paths/circuits. Once a first series of cuts are created, the hypotube is coated with an electrically isolating material, such as parylene, which also acts to bond the circuit paths where the laser cut was made. Parylene strikes a balance between conformal coating properties and high tensile strength, however other materials exhibiting similar characteristics may also be used. Additional laser cuts can be further made to complete any necessary electrical/circuit paths. The parylene insulation may also help hold the hypotube together, thus the circuit cuts are completed after the insulation is added to the preliminary circuit cuts. Once the circuit route is completed, another round of Parylene coating is undertaken to fully encapsulate the component. A final laser cutting process is undertaken where the coating is removed or ablated at key locations in order to allow for the addition of additional wires as resistors within the circuit paths. The hypotube 30 in this form functions in a similar manner to a traditional printed circuit board.

[0053] The hypotube circuit can be used for a number of purposes. For example, components can be added to the hypotube 30 itself to allow for signal conditioning or processing at the site of an electrical components instead of at the user interface. In one example, small wires of various resistive properties can be added to create a Wheatstone bridge to increase sensor accuracy. An operational amplifier could also be integrated on the hypotube circuit 25 to improve sensor values.

[0054] A wire (e.g., a catheter structural braid wire 18) connects the sensor to the proximal user interface to relay the signal. Much of the signal processing or signal

conditioning could be done on the hypotube circuit itself through the methods discussed. Alternatively or additionally, signal processing could also be done on the user interface.

[0055] The hypotube 30 may also include a number of signal processing elements, such as operational amplifiers, signal filtering, etc. as part of the circuit 25. One advantage of doing the signal processing in the hypotube 30 itself instead of in the user interface 16 is that the user interface resources could be freed up for other purposes. Additionally, since signals may degrade when conveyed over a distance, the signal can be cleaned up at the distal part of the system before being sent back to the user interface 16, thus reducing the effect of signal degradation on system operation.

[0056] One advantage of the circuit concept, as described earlier, is that the circuit 25 and its connection to one or more of the electrical components 26 is completed at the distal portion 11A of the catheter 10, instead of allowing each of the electrical components 26 to have its own wires 18 connected to the interface 16. Hence, the catheter tube 11 may be formed to have a relatively smaller outer diameter.

[0057] The electrical components 26 may be used for a number of functions, such as an imaging system, pressure sensing, temperature sensing, oxygen sensing, or any number of additional systems used with powered catheters/microcatheters. The electrical components may also be used as part of an embolic coil detachment system, and/or a detachable catheter tip system, and/or a steerable guidewire system.

[0058] Figure 7 and 8 illustrate an alternate structure for a hypotube 32, similar to that of the hypotube 30. In this respect, the hypotube 32 includes one or more notches 32A and a plurality of elongated finger contacts 32B that are each angled or bent inwardly into the hypotube 32. In this respect, power can be supplied to the contacts 32B which, when in contact with electrical contacts on an inner catheter or pusher can cause the catheter or pusher to perform a function, such as detach an implant via a heater or mechanical mechanism.

[0059] Figures 9A and 9B illustrate one example use of a hypotube 32 having contacts 32B used to detach an embolic coil 42 similar to that disclosed in U.S. App. 14/578,106, which is hereby incorporated by reference. The hypotube 32 includes a distal power terminal 20 and a proximal terminal 22 that are connected to one or more distal or proximal

contacts 32B, respectively. The embolic coil 42 has one or more detachment points 44 at select locations along the coil 42. When the electrical contacts 32B align with the embolic coil 42 and the detachment point 44 the interface 16 may indicate or display the alignment. Once the user has received an alignment signal, a desired action can be actuated, such as pressing a button to initiate detachment of the coil 42 at the detachment zone 44 from the pusher 40. Since the hypotube 32 can support multiple electrically powered components, a sensor 32C may also be included on the hypotube 32, providing functionality such as detachment detection, temperature sensing, or imaging.

[0060] Figures 10 and 11 illustrate a more specific example of the detachment point 44 of the embolic coil. Two conductive cylinders or sleeves 54 and 55 are mated to a proximal and distal end of an insulating sleeve 56 via adhesive or glue. The conductive sleeves 54 and 55 are composed of a conductive material, such as a 92/8 ratio platinum/tungsten material.

[0061] Heater 60, which can be a coil of wire, spans the area between the proximal and distal conductive sleeves 54 and 55, connecting its ends to each of the sleeves, allowing current to pass through each of the components. Hence, when properly aligned with the proximal and distal contacts 32B of the hypotube 32 and current is applied, the heater coil 60 will increase in temperature, melting the adhesive of the insulating sleeve and causing the distal portion of the embolic coil 42 to detach. Springs 57 and 58 allow for attachment of a monofilament or tether to help prevent stretching of the embolic coil. In an alternate embodiment, a tether may connect between the two springs 57, 58 so as to hold the two segments of the embolic coil 42 together and therefore can be broken by the heater 60 to cause detachment.

[0062] In another one example similar to that disclosed in 14/578,106, a steerable guidewire system utilizes spaced positive and negative electrical contacts on a hypotube, similar to that describe in Figures 9A and 9B which electrically interact with a bimetallic guidewire to angle a distal end of the guidewire to enable navigation of the guidewire through the vasculature.

[0063] As previously discussed, the hypotube 30 and its circuitry can be used to power a heater coil in the catheter 10. In one example Figures 12 and 13 disclose a catheter 10

having a detachable distal end tip 11A that is similar to the embodiments disclosed in U.S. App. 14/578,020 and hereby incorporated by reference. The hypotube 30 is located at a distal portion of the elongated tubular portion 11 and an adhesive 48 maintains the distal end tip 11A to the elongated tubular portion 11. The user can initiate a detachment sequence (e.g., push a button on the interface 16) to activate the heater 49 and melts the adhesive 48 to effect detachment of the distal end tip 11A of the microcatheter 10 for various reasons (e.g., during delivery of a liquid embolic where there is danger of the distal tip 11A of the catheter getting glued into the vasculature). Similar to the previous example, the hypotube 30 connects to the braided structural wires 18 and provides electrical pathways to the heater 49. In this example, the heater 49 may be located adjacent to or even be connected to the inner surface of the hypotube 30.

[0064] Figure 14 illustrates an alternate embodiment of the hypotube 30 of Figure 13, but instead of connecting to a single heater 49, the hypotube 30 connects to a proximal heater coil 49A, a middle heater coil 49B, and a distal heater coil 49C. The hypotube 30 can be connected to three discrete pairs of wires 18 and electrical paths on the hypotube 30, allowing each of the heater coils to be individually activated.

[0065] Figure 15 illustrates a hypotube 30 with multiple heater coils 49, similar to that of Figure 14, except that the coils are located parallel and adjacent to each other. In this regard, the hypotube 30 may be located either in a catheter or within a pusher sized for movement within a catheter.

[0066] Alternately, the user interface may contain multiple batteries, allowing multiple terminal banks on the hypotube which are connected to the multiple batteries. In another alternative, multiple batteries are used, allowing one battery to provide the terminal bank and the other batteries are selectively used for particular systems (i.e. one battery solely used to power the terminals for the variable coil detachment system, and/or one battery solely used to power the terminals for the detachable tip catheter system). Thus, for example, there could be one positive contact and two negative contacts spaced out at different intervals to interact with the different systems. Similarly, there may be one negative contact and two positive contacts spaced apart at different intervals to interact with the different systems. In one example, the electrical components could control the operation of the exact system in use (i.e. variable detachment, detachable tip, steerable

guidewire, or another system) via the integrated circuitry on the hypotube and the signal which is sent to the user interface via the wire braid, as discussed earlier. In another example, the distal hypotube electrical components would be unnecessary if the braid wires are solely used to convey current from the battery as opposed to a signal from electrical components. In this example, the user interface itself would have the circuitry for the various systems and the wires which are used to convey the current between the proximal and distal ends of the catheter are also used to convey the signal from the user interface (i.e. convey the signal input to detach the embolic coil, or detach the catheter tip, or deflect the guidewire tip).

[0067] The embodiments and systems described herein offer many advantages in creating a powered catheter system. The following is a non-exhaustive list. One of the main advantages of the system is using the catheter braid itself to convey current, thus providing a useful secondary benefit to the catheter braid besides structural reinforcement of the catheter. Another advantage of the system is using two of the catheter braid wires to power the terminal banks on the hypotube at the distal end of the catheter, and having the electrical components directly connect to the terminal banks on the hypotube itself, thus only requiring one wire to connect the electrical components to the user interface since the electrical components are powered on the hypotube itself. Another advantage of the system is utilizing the distal hypotube as a circuit system, and the ability to allow signal processing to be done on the hypotube itself via the integrated circuitry, instead of at the proximal end of the system. Signals can degrade over a long distance, so offering signal processing at the source of the signal offers some advantages in and of itself. Another advantage is the ability to combine several powered catheter functionalities without requiring a large number of wires to convey all the signals.

[0068] In other embodiments, the system described herein would not need a separate negative terminal source and the patient himself could be used as the ground to complete the circuit. Thus, in one example, the proximal part of the system would just contain a positive charge source, a wire would run the current to the distal end of the system and the patient himself would comprise the ground. The distal end of the system would still utilize all the circuitry with the electrical components, but this would allow for an additional

electrical component since only one wire would be needed to convey the current since the patient provides the ground.

[0069] In other embodiments, an alternate current voltage source could be used instead of a direct current voltage source.

[0070] In other embodiments, the wiring for the catheter system would not utilize a catheter braid (i.e. if the catheter does not utilize any braiding) but consists of wires which are external or internal to the catheter surface, or integral between layers of the catheter tubing. In other embodiments reinforcement coil(s) or ribbon(s) could be used instead of a braid.

[0071] In other embodiments the terminal banks could be replaced with a capacitor. The capacitor could then store the charge from the voltage source.

[0072] The embodiments described include a circuit system. The circuit system can be used on a number of devices including interventional devices, including a catheter or microcatheter or other delivery device.

[0073] The embodiments described utilize the structural reinforcement layer of a catheter (generally described as a braid) to conduct current between two ends of the catheter. Though the term braid is used, the term should be interpreted broadly so as to describe any structural layer, thus the term braid may include coils, ribbons, and other structural components commonly used in catheters.

[0074] Although the invention has been described in terms of particular embodiments and applications, one of ordinary skill in the art, in light of this teaching, can generate additional embodiments and modifications without departing from the spirit of or exceeding the scope of the claimed invention. Accordingly, it is to be understood that the drawings and descriptions herein are proffered by way of example to facilitate comprehension of the invention and should not be construed to limit the scope thereof.

What is claimed is:

1. A catheter comprising:
 - an elongated tubular portion having a proximal end and a distal end;
 - a plurality of wires extending between said proximal end and said distal end;
 - a hypotube located at said distal end of said elongated tubular portion; said hypotube comprising a plurality of electrical paths connected to one or more of said plurality of wires;
 - one or more electrically powered components connected to said hypotube and in electrical communication with one or more of said electrical paths; and,
 - an interface connectable to said proximal end of said elongated tubular portion to supply power to said hypotube via at least two of said plurality of wires.
2. The catheter of claim 1, wherein said hypotube is composed of a gold plated polyimide.
3. The catheter of claim 1, wherein said electrical paths on said hypotube are shaped by laser cutting said hypotube.
4. The catheter of claim 1, wherein said hypotube further comprises a positive terminal bank region and a negative terminal bank region.
5. The catheter of claim 4, wherein said one or more electrically powered components is a plurality of electrically powered components that are each connected to said positive terminal bank region and said negative terminal bank region.
6. The catheter of claim 1, wherein said one or more electrically powered components is selected from an imaging sensor, pressure sensor, temperature sensor, and oxygen sensor.
7. The catheter of claim 1, wherein said one or more electrically powered components is selected from a heater or a mechanical latch system.

8. The catheter of claim 1, wherein said hypotube further includes a circuit.
9. The catheter of claim 8, wherein said circuit is a Wheatstone bridge.
10. The catheter of claim 8, wherein said circuit is an amplifier.
11. The catheter of claim 1, wherein said hypotube includes a plurality of electrical contacts located along an interior of said hypotube.
12. A catheter comprising:
 - an elongated tubular portion having a proximal end and a distal end;
 - a hypotube located at said distal end of said elongated tubular portion and forming one or more electrical paths;
 - one or more electrically powered components connected to said hypotube and in electrical communication with one or more of said electrical paths; and,
 - an interface connectable to said proximal end of said elongated tubular portion to supply power to said hypotube via at least two of said plurality of braided wires.
13. The catheter of claim 12, further comprising a plurality of braided structural wires supporting said elongated tubular portion, said braided structural wires electrically connected to said hypotube and to an interface at a proximal end of said catheter.
14. The catheter of claim 12, wherein said one or more electrically powered components is selected from an imaging sensor, pressure sensor, temperature sensor, and oxygen sensor.
15. The catheter of claim 12, wherein said one or more electrically powered components is selected from a heater or a mechanical latch system.

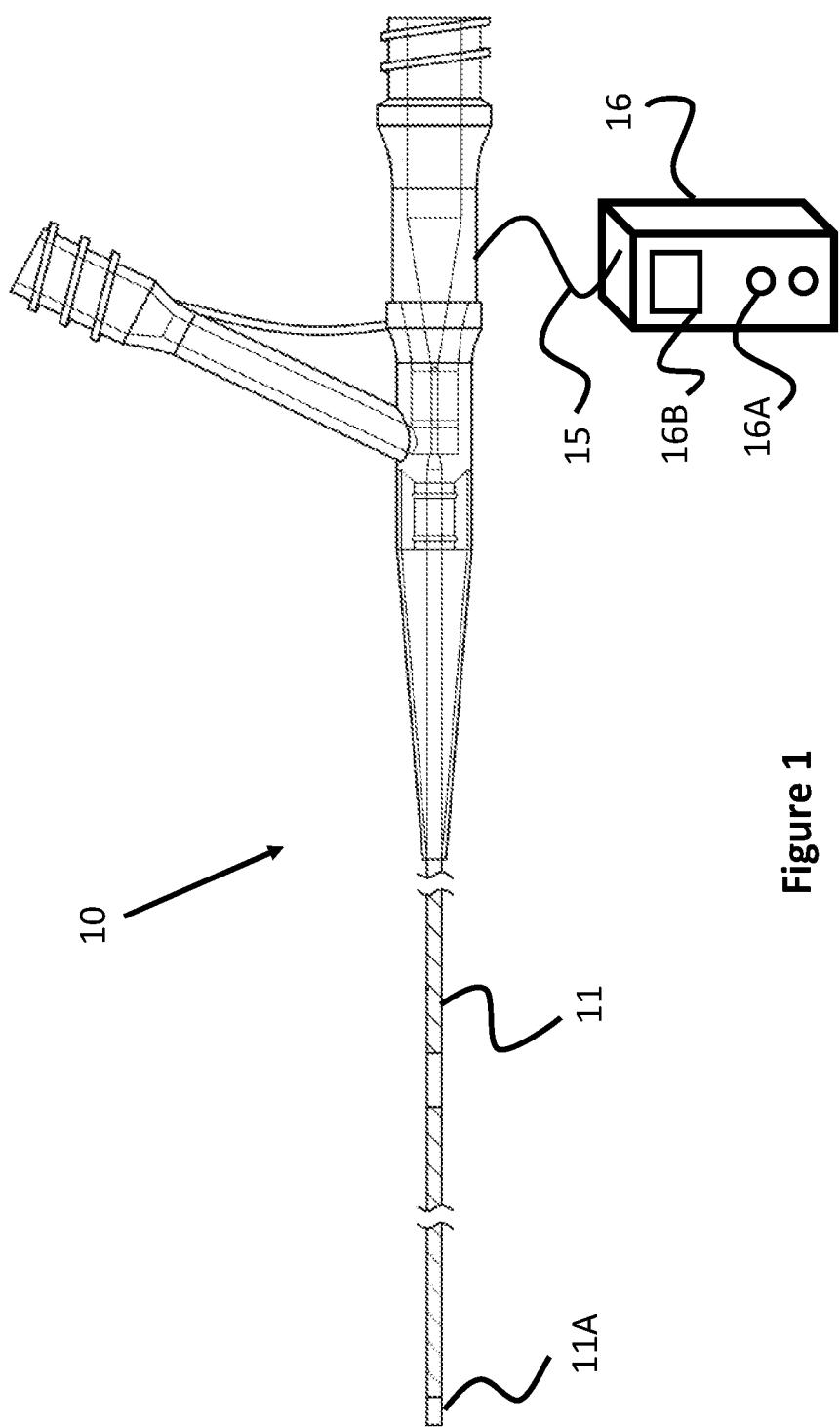


Figure 1

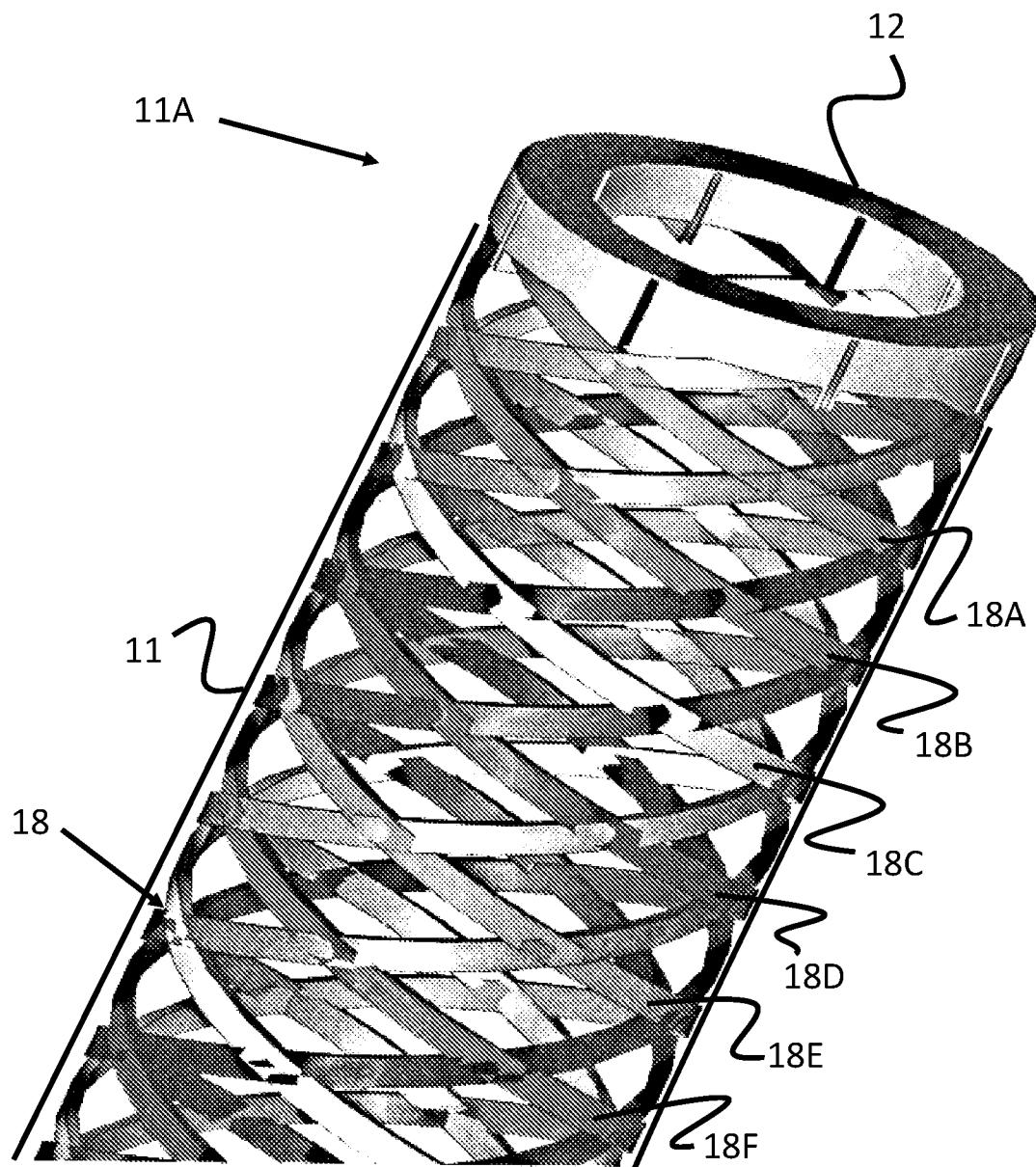


Figure 2

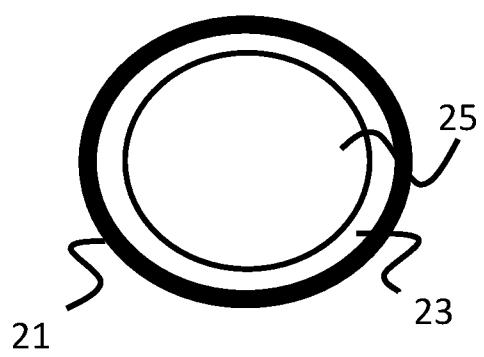


Figure 3A

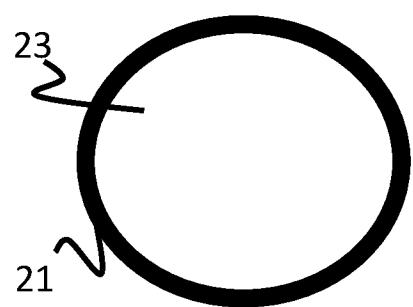


Figure 3B

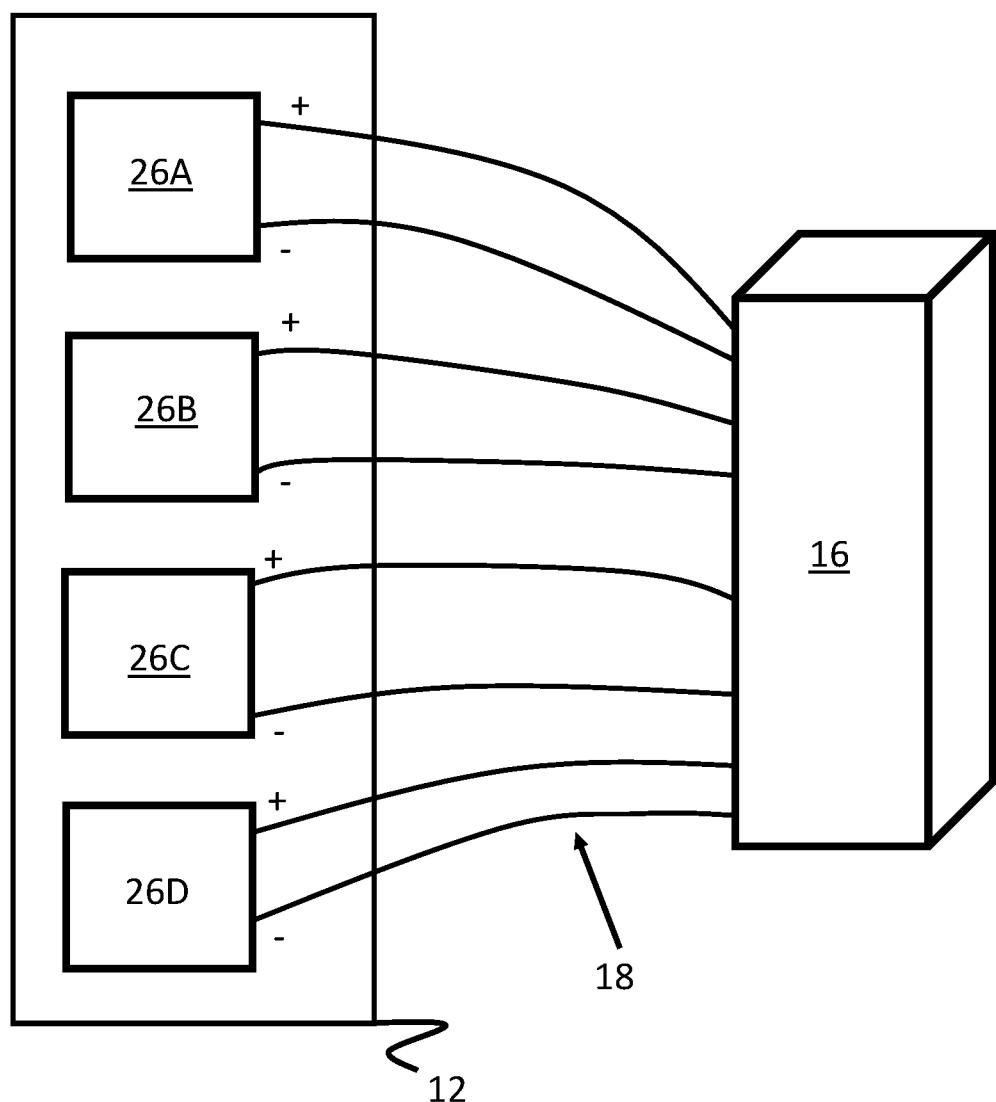


Figure 4

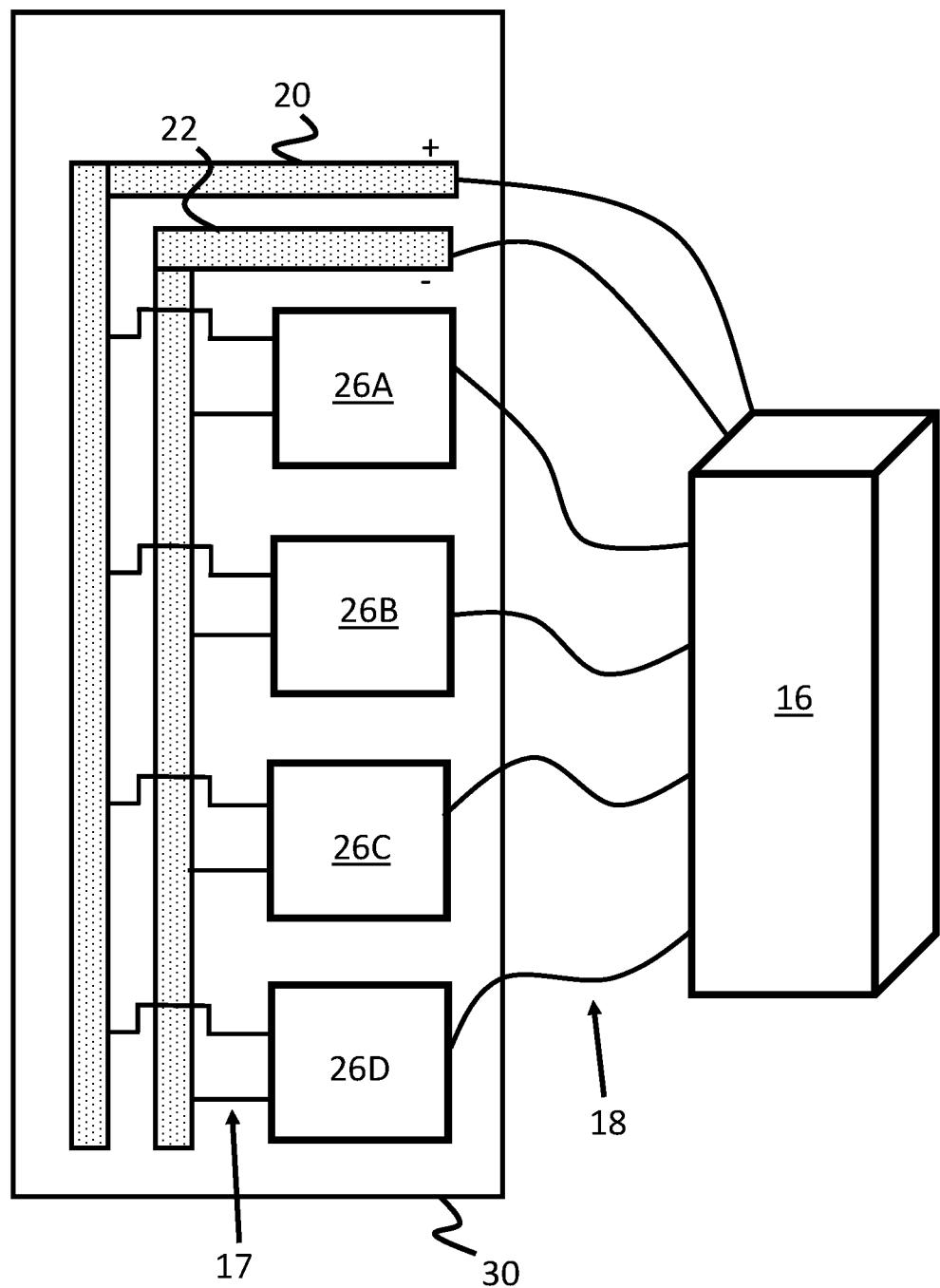


Figure 5

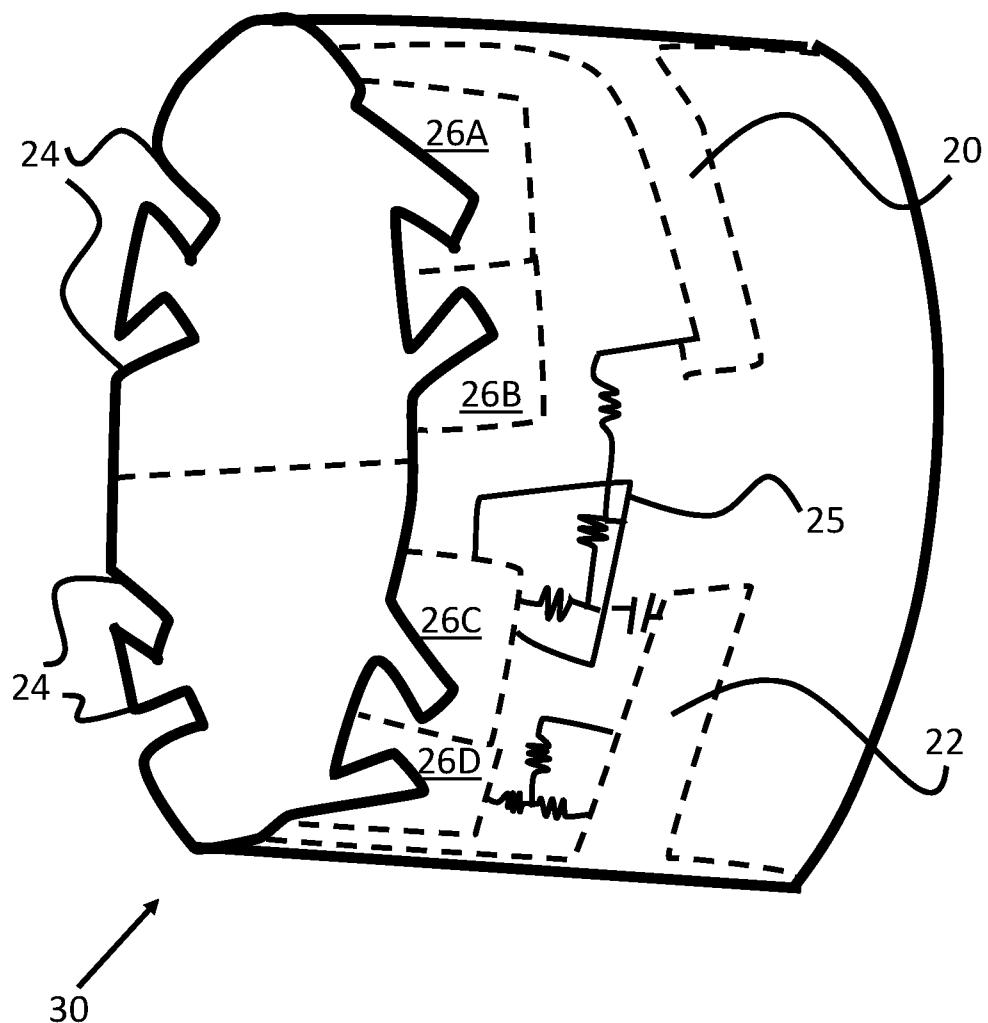


Figure 6

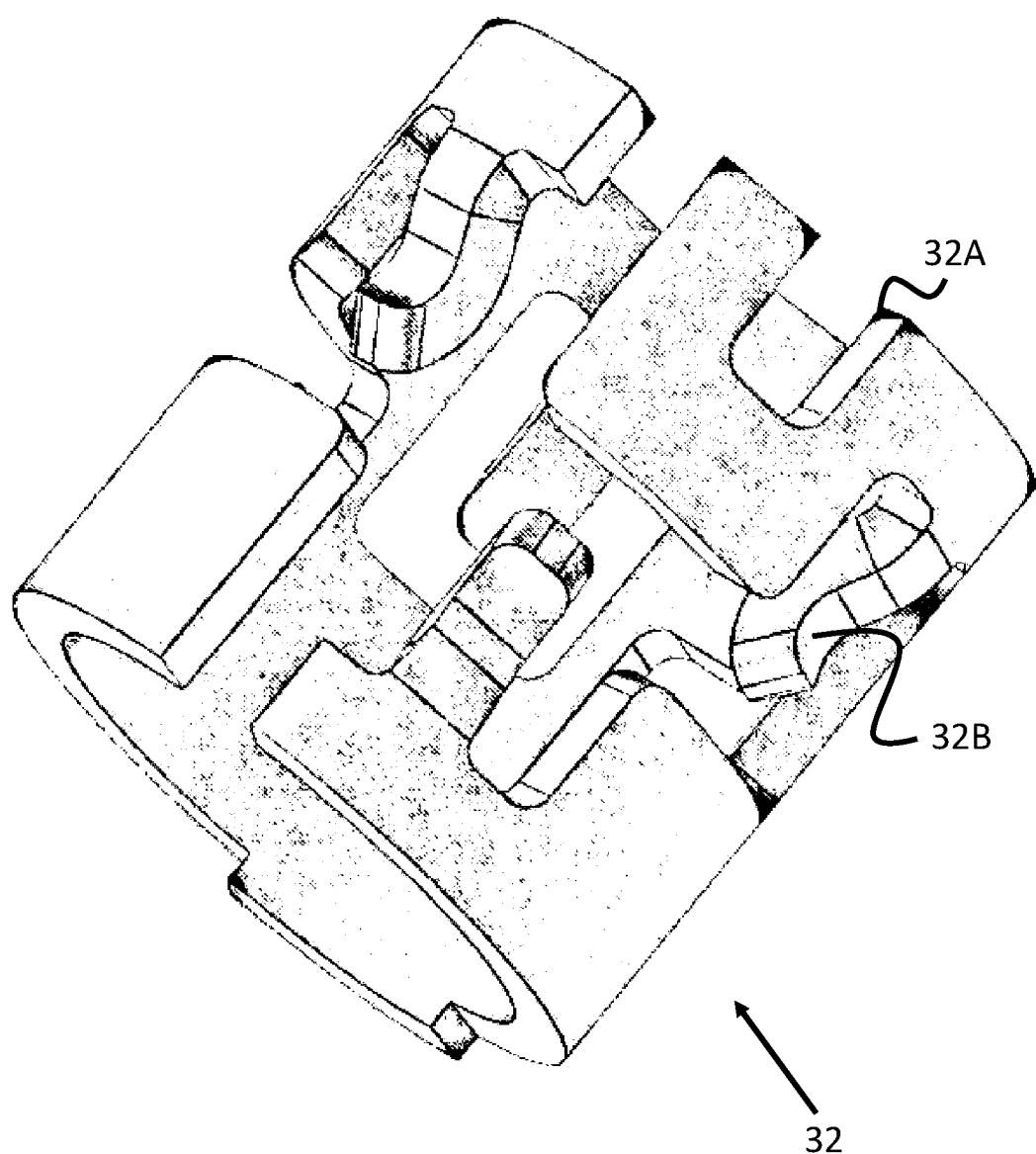


Figure 7

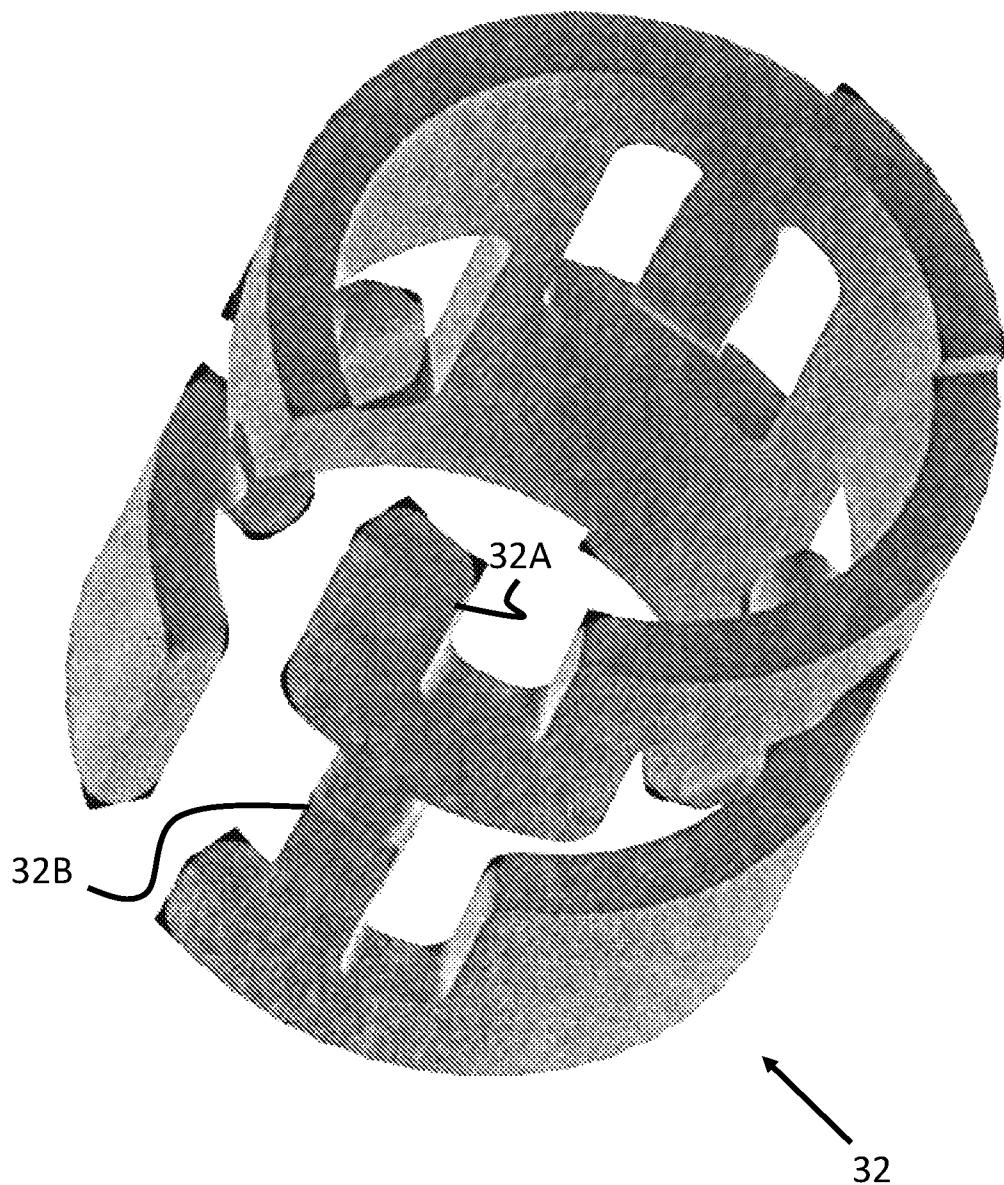


Figure 8

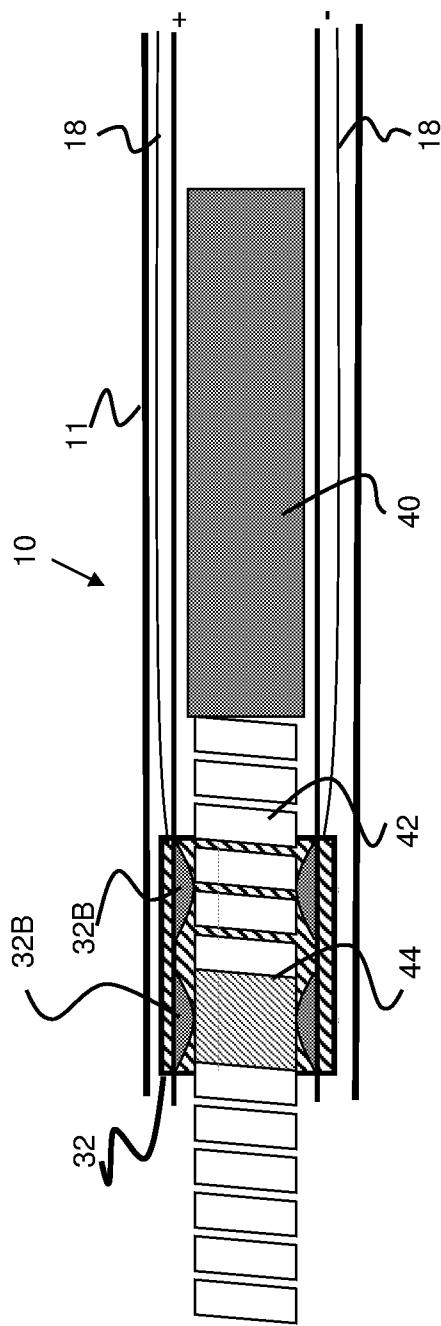


Figure 9A

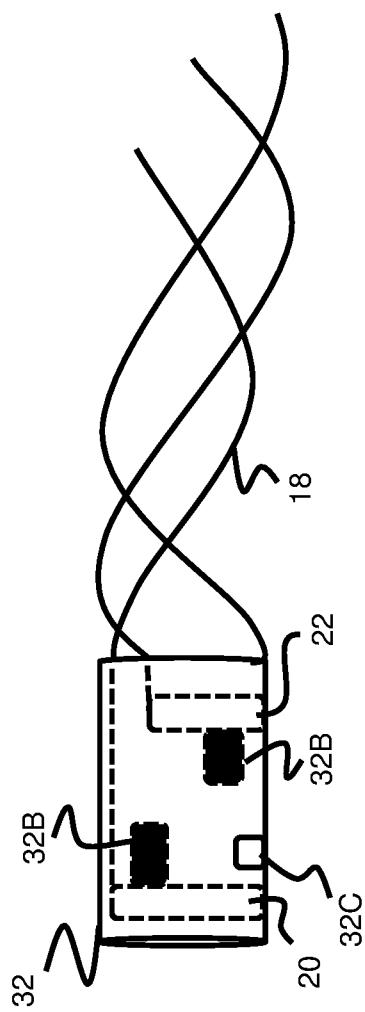


Figure 9B

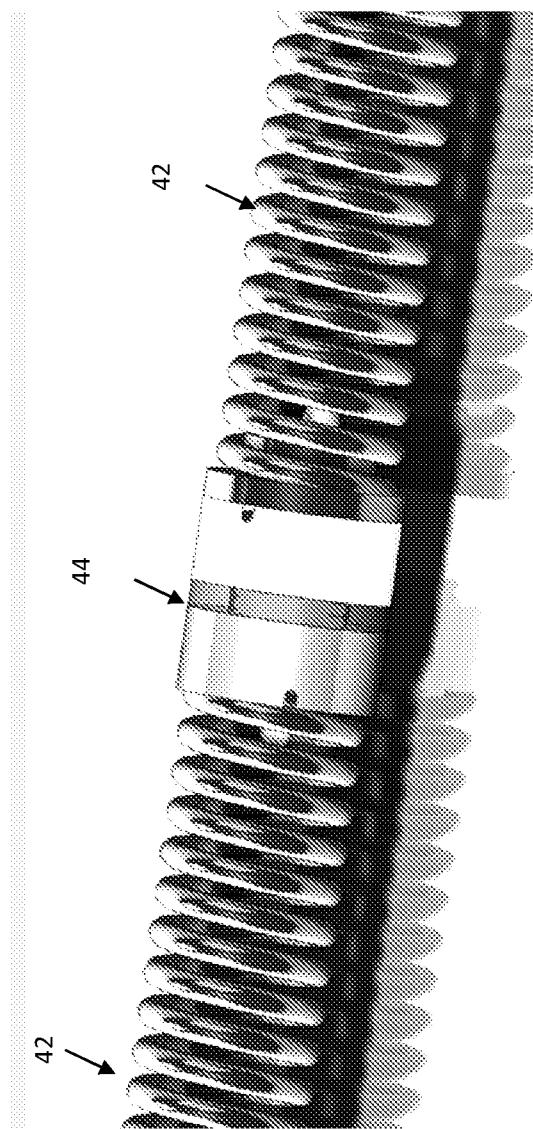


Figure 10

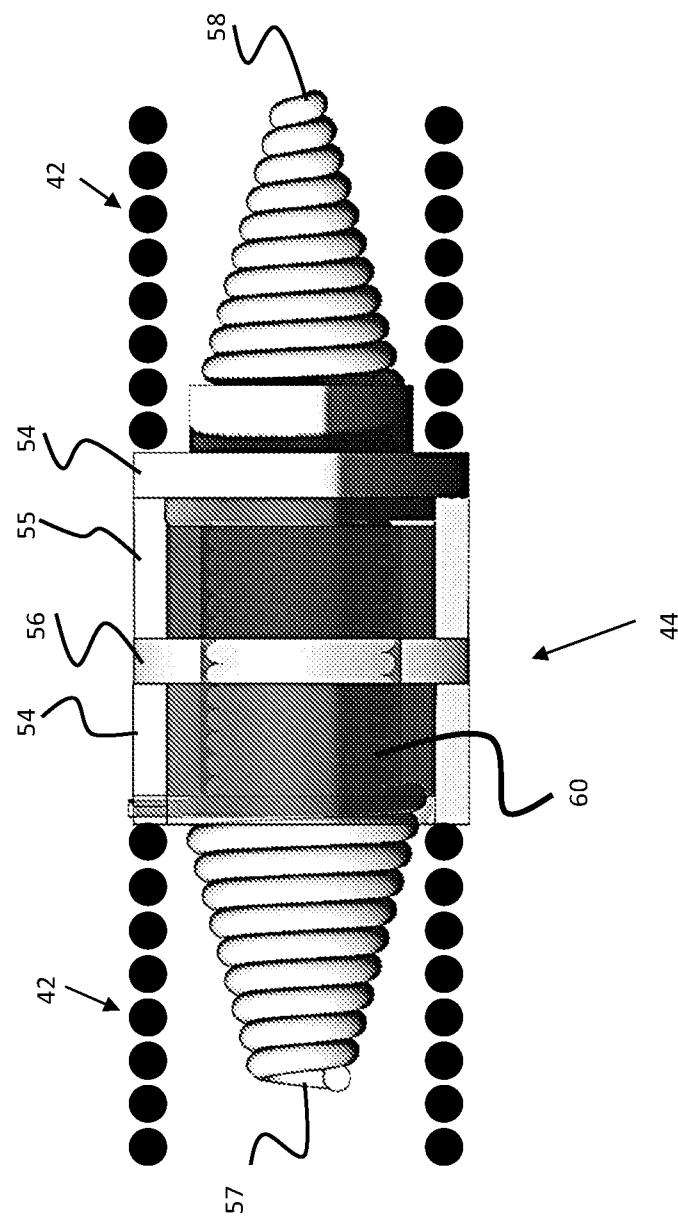
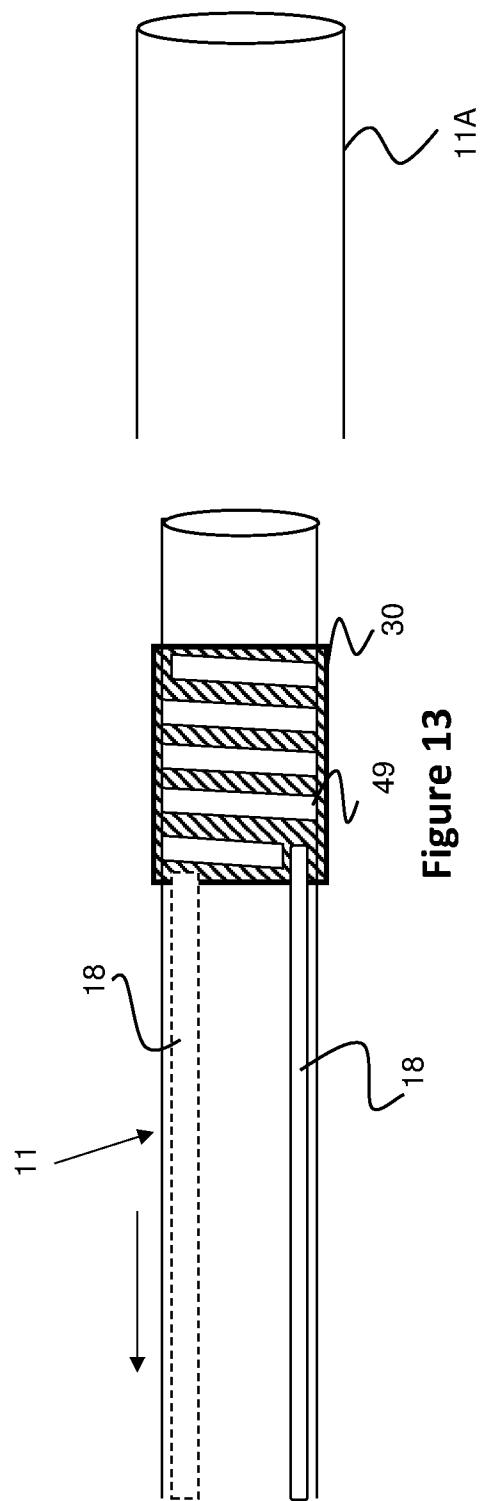
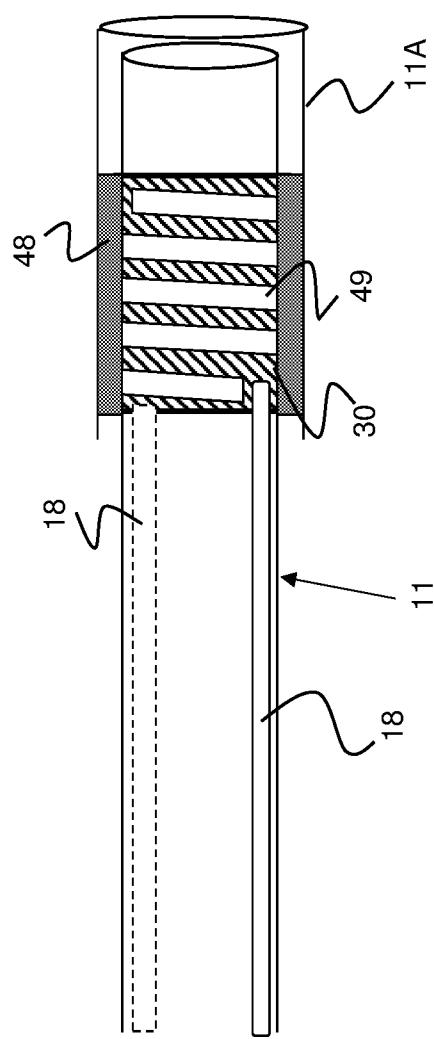


Figure 11



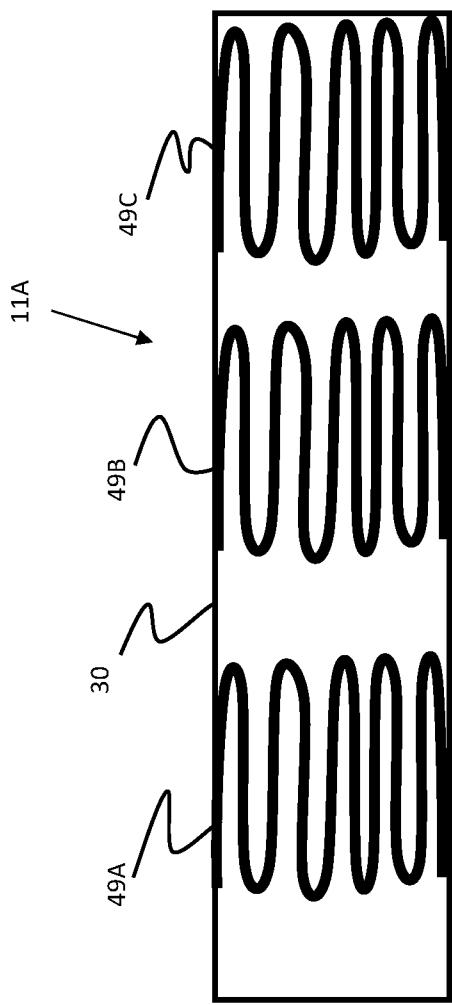


Figure 14

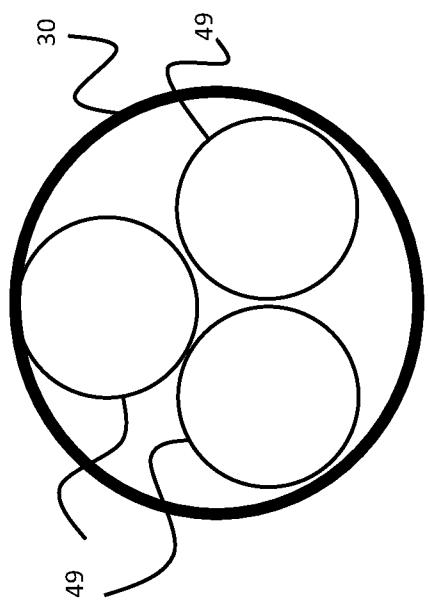


Figure 15

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 16/35106

A. CLASSIFICATION OF SUBJECT MATTER

IPC(8) - A61M 25/16 (2016.01)

CPC - A61M 25/005, 25/0051

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC(8) : A61M 25/16 (2016.01)

CPC : A61M 25/005, 25/0051

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

IPC(8) : A61M 25/00, A61B 5/00, 5/02, 5/04, 5/145, 5/1459, 5/1473 (2016.01)

CPC: A61M 25/00, 2025/0001, 25/0009, 25/0012, 25/0043; A61B 5/00, 5/02, 5/04, 5/145, 5/1459, 5/1473

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
Patbase, Google Patent, Google Scholar: sensor, catheter, hypotube, electrical, conductive, power, path, trace, positive, terminal, bus, bank, negative, return, ground, gold, polyimide, component, substrate, support, laser, cut, heater, hotwire, braid, wire, plated, mount, etched

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 2003/0222325 A1 (JACOBSEN et al) 04 December 2003 (04.12.2003) see especially para [0055]-[0058], [0065], [0072], [0082], [0097], fig 1-3	1-15
Y	US 2005/0091833 A1 (KIEPEN et al) 05 May 2005 (05.05.2005) see especially para [0024], [0029], [0030], [0032], fig 7, 9	1-15
Y	US 2006/0074318 A1 (AHMED et al) 06 April 2006 (06.04.2006) see especially para [0066]	3
Y	US 4,274,423 A (MIZUNO et al) 23 June 1981 (23.06.1981) see especially col 4, ln 24-65, col 7, ln 8-38, fig 10a, 10b	9-10
Y	US 5,591,142 A (VAN ERP) 07 January 1997 (07.01.1997) see especially col 1, ln 52 to col 2, ln 3, col 3, ln 6-28, col 3, ln 38-58, fig 3	12-15
A,P	US 2015/0173773 A1 (BOWMAN et al) 25 June 2015 (25.06.2015) see whole document	1-15
A	US 2010/0057174 A1 (HARRISON et al) 04 May 2010 (04.05.2010) see whole document	1-15
A	US 5,555,618 A (WINKLER) 17 September 1996 (17.09.1996) see whole document	1-15
A	US 4,484,586 A (McMICKLE et al) 27 November 1984 (27.11.1984) see whole document	1-15

Further documents are listed in the continuation of Box C.

* Special categories of cited documents:

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- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

- "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
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- "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
- "&" document member of the same patent family

Date of the actual completion of the international search

21 July 2016

Date of mailing of the international search report

30 AUG 2016

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