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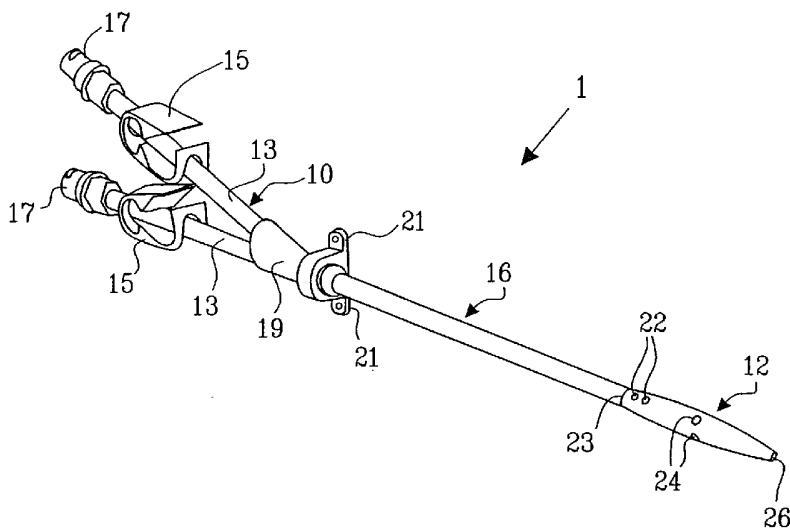
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(54) Title: MULTILUMEN VASCULAR CATHETER AND METHOD FOR MANUFACTURING THE SAME



(57) Abstract: A multilumen vascular catheter (1) for treatment of patients by insertion of said vascular catheter (1) in a venous blood vessel (14) by means of a guide-wire (28), said vascular catheter (1) comprising:
- a proximal connection portion (10);
- a distal end-portion (12) which is terminated with in a guide-wire opening (26);
- a flexible catheter tube (16) arranged between the proximal connection portion (10) and the distal end-portion (12), said catheter tube (16) comprising a first lumen (18) for extraction of fluid such as a.9 for example untreated blood from the vessel (1) and a second lumen (20) for introducing fluid such as for example treated blood to the blood vessel (14);
- one or more suction openings (22) communicating with said first lumen

(18), said suction openings (22) being located upstream of one or more outlet openings (24), which in turn communicate with said second lumen (20), said suction openings (22) and outlet openings (24) being located at said distal end-portion (12). The invention is especially characterized in: - that the distal end-portion (12) is permanently bulbous and exhibits a first, widening section (A) starting from the catheter tube (16) with a gradually increasing external cross-section in the direction towards said guide-wire opening (26), said first section (A) transiting downstream via a shoulder (30) with a maximum external diameter into a second, narrowing section (B) having a gradually decreasing external cross-section in the direction towards the guide-wire opening (26), and - that said one or more suction openings (22) are located in the first, widening section (A) of said distal end-portion (12), whilst said one or more outlet openings (24) are located in the second, narrowing section (B) of said distal end-portion (12).

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5 MULTILUMEN VASCULAR CATHETER AND METHOD FOR MANUFACTURING THE SAME

TECHNICAL FIELD

The present invention refers to a multilumen vascular catheter for treatment of patients by insertion of said vascular catheter in a venous blood vessel by means of a
10 guide-wire. The vascular catheter comprises a flexible catheter tube arranged between a proximal connection portion and a distal end-portion. The catheter tube in turn comprises a first lumen for extraction of fluid such as for example untreated blood from the vessel and a second lumen for introducing fluid such as for example
15 treated blood to the blood vessel.

BACKGROUND

Vascular catheters form very important components in modern medical treatment systems within, for example, blood dialysis treatment and intensive care. Vascular catheters of a so called multilumen type having two or more parallelly extending,
20 mutually separated lumina, are since long well-known in the art. In, for example, blood dialysis, a first lumen is used as a conduit for blood flowing out of a dialysis patient to an external dialysis device, whilst a second lumen is used as a conduit for treated blood flowing from the dialysis device and back into the dialysis patient. Multilumen catheters are preferable before single lumen catheters, since they
25 eliminate the need for several separate catheters, whereby the discomfort of the patient and the risk of infection upon insertion of the catheter are both reduced.

Vascular catheters of the above described type, are normally inserted by means of the so called Seldinger method, named after the inventor Seldinger, who in the
30 1950's introduced an insertion method for vascular catheters, in which a hollow syringe is first used to puncture a blood vessel, whereafter a flexible guide-wire is inserted through the syringe and further into the blood vessel to a desired position. The syringe is then removed and the catheter is guided via one of its lumen, over the guide-wire and into a desired position in the blood vessel of the patient, whereafter
35 the guide-wire is retracted. The positioning in the blood vessel is normally supervised by means of ultrasound technology or other tissue scanning technology. In English language branch literature, the guide-wire is sometimes named after the inventor as a "Seldinger guide-wire", or a "Seldinger-wire".

Vascular catheters are further provided, at a distal end-portion or "tip" with one or more suction openings communicating with the first lumen as initially mentioned under the title TECHNICAL FIELD. The suction openings are located upstream – with
5 reference to the flow direction of the blood vessel – of one or more outlet openings, that in turn communicate with said second lumen. Normally, the suction openings and the outlets openings are located relatively close to each other and are thereby normally both located at or in close proximately to the distal end-portion of the vascular catheter.

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One example of a known multilumen vascular catheter is described in the US patent specification US-6,206,849 B1 (Martin et al). This vascular catheter comprises, except for a first outlet lumen and a second inlet lumen, also a central, separately formed third lumen designated for the guide-wire and eventual subsequent
15 intravenous supply of medical substances. The distal end-portion is formed as a first, upstream, circular-cylindrical section in which the suction openings and outlet openings are located, and a thereafter following, downstream conical terminal section. This general outer design of the distal end-portion of the vascular catheter can be found on several of the vascular catheters that are now available on the
20 market.

A potential problem with the common design of the distal end-portion described above is, however, that a certain undesired recirculation may occur between the downstream outlet openings and the upstream suction openings. Part of the treated
25 blood meant to be brought back to the blood vessel is then sucked back into the suction openings for untreated blood, resulting in a reduced treatment effect. The risk for such a recirculation is particularly increased at high flow speeds through the vascular catheters, since the suction effect from the suction openings is then stronger than cases with lower exchange flows. High flows in vascular catheters are,
30 however, getting increasingly common within modern healthcare, due to demands for quicker treatment cycles in order to achieve a more effective patient treatment and a reduction of the patient's discomfort.

Another problem with many known vascular catheters is that they sometimes tend to
35 adhere to the vascular wall by suction, whereby the suction openings – and sometimes also the outlet openings – are fully or partially blocked, resulting in a reduced flow through the vascular catheters. At high flows, this situation may give rise to injuries or irritations on the vascular wall, particularly when the catheter is in

use for a longer period. Depending on the curvature of the blood vessel, local asymmetric restrictions, etc., the vascular catheter is normally not centered in the blood vessel during use and its distal end-portion may therefore already in an initial stage be pressed against the vascular wall in such a way that the suction openings and/or the outlet openings are blocked. In the above described known vascular catheter according to US-6,206,849 B1 (Martin et al), both the suction openings and the outlet openings are formed in the circular-cylindrical, "straight" section of the distal end-portion, which should further increase the tendency of the vascular catheter to adhere by suction to the vascular wall. In the US-patent specification US-6,280,423 B1 (Davey et al), a way to design the distal end-portion of the vascular catheter so as to minimize the tendency to adhere by suction to the vascular wall during use, is described. According to this document, the problem is solved by orientating a suction opening (reference 35 in Fig. 3a and Figure 3b of the document) perpendicularly to the direction of flow in the blood vessel, a distance upstream of a terminal outlet opening (37). A guide-body (202) is placed downstream of the suction opening and at a certain distance from it, whereby a recess (202) for the suction opening is formed. By recessing the suction opening in this way, it cannot be blocked by direct abutment to the vascular wall. Even if this design of the distal end-portion minimizes the tendency of the vascular catheter to adhere by suction to the vascular wall, the deep recess (202) and the abrupt dimensional changes result in an undesired flow situation around the distal end-portion, which may, for example give rise to undesired build-up of trailing formations of coagulated blood.

25 **SUMMARY OF THE INVENTION**

The above mentioned problem is solved by the invention providing a multilumen vascular catheter which effectively prevents undesired recirculation between outlet openings and suction openings, at the same time as the tendency for the catheter to adhere by suction to the vascular wall is minimized. This has been achieved by a novel design of the distal end-portion of the vascular catheter, according to the appended claim 1.

Thus, the invention provides a multilumen vascular catheter for treatment of patients by insertion of said vascular catheter in a venous blood vessel by means of a guide-wire, said vascular catheter comprising:

- a proximal connection portion;
- a distal end-portion which is terminated with a guide-wire opening;

- a flexible catheter tube arranged between the proximal connection portion and the distal end-portion, said catheter tube comprising a first lumen for extraction of fluid such as for example untreated blood from the vessel and a second lumen for introducing fluid such as for example treated blood to the blood vessel;

- 5 - one or more suction openings communicating with said first lumen, said suction openings being located upstream of one or more outlet openings, which in turn communicate with said second lumen, said suction openings and outlet openings being located at said distal end-portion.

The invention is especially characterized in:

- 10 - that the distal end-portion is permanently bulbous and exhibits a first, widening section starting from the catheter tube with a gradually increasing external cross-section in the direction towards said guide-wire opening, said first section transiting downstream via a shoulder with a maximum external diameter into a second, narrowing section having a gradually decreasing external cross-section in the
15 direction towards the guide-wire opening, and
- that said one or more suction openings are located in the first, widening section of said distal end-portion, whilst said one or more outlet openings are located in the second, narrowing section of said distal end-portion.

- 20 In an advantageous embodiment of the invention, said first, widening section, as well as said second, narrowing section of said distal end-portion exhibit a substantially conical shape.

- 25 In a well functioning embodiment, both the first, widening section and the second, narrowing section of said distal end-portion exhibit a rounded conical shape, in such a way that the shoulder forms a rounded transition between the two sections.

- 30 In one embodiment, said one or more outlet openings are located adjacent to the shoulder, at an axial distance from said shoulder corresponding to between 5-20% of the length of the second, narrowing section.

- 35 Said one or more suction openings are preferably located adjacent to a narrow end of the first, widening section of the distal end-portion, at one or more axial distances from said narrow end corresponding to between 5-20% of the length of the first, widening section.

In a favorable embodiment, the shoulder has an external cross-section exceeding the diameter of the catheter tube by 10-20%.

In one embodiment, the first, widening section of the distal end-portion, in its internal periphery, exhibits an internal cylindrical recess shaped to receive a corresponding end-portion of the catheter tube, said internal cylindrical recess being limited in the axial direction of the widening section, by a radial abutment edge adapted for abutment against a square-ended terminal end of the end-portion of the catheter tube.

In a favorable embodiment, the distal end-portion, downstream of the internal cylindrical recess, exhibits a cylindrical bore, the internal diameter of which corresponds to the internal diameter of the catheter tube, said bore extending continually from the first, widening section into the second, narrowing section of said distal end-portion.

In an embodiment well suited for production, an end plug is inserted into said first lumen at the square-ended terminal end of the end-portion of the catheter tube, said end plug being arranged to prevent communication between said first lumen and said second lumen. The end plug exhibits an abutment surface for abutment against said square-ended terminal end of the end-portion of the catheter tube, a portion of the end plug extending upstream from said abutment surface into said first lumen to a suction opening.

In a favorable embodiment, the end plug extends downstream into said cylindrical bore, and further on to – or just upstream of – one of said outlet openings.

Suitably, the end plug exhibits a first upstream, doubly arced and upstreamingly slanted end surface forming a smooth transition between said first lumen and at least one of said suction openings.

Correspondingly, the end plug exhibits a first downstream, doubly arced and downstreamingly slanted end surface forming a smooth transition between said second lumen and at least one of said outlet openings.

The invention also discloses a method for producing a multilumen vascular catheter, whereby the end plug is first mounted in said first lumen in such a way that its abutment surface abuts the square-ended terminal end (40) of the end-portion (36) of the catheter tube, whereinafter the distal end-portion is mounted on the end-

portion of the catheter tube, said mounting of said parts being effected by welding and/or by gluing. Preferably, said parts are welded together in a single welding step.

Further features and advantages of the invention will be described in the detailed
5 description of embodiments below.

BRIEF DESCRIPTION OF THE DRAWINGS

10 The invention will now be described in greater detail by way of example only and with reference to the attached drawings, in which

- Fig. 1 shows a perspective view of a vascular catheter according to an
embodiment of the invention;
- 15 Fig. 2 shows a schematical elevational cross-sectional view through the distal end portion of the vascular catheter, shown inserted in a venous blood vessel;
- 20 Fig. 3 shows a perspective "X-Ray"-view of the distal end-portion of the vascular catheter, illustrating the positions of suction openings and outlet openings in a suitable embodiment;
- 25 Fig. 4 shows a cross-sectional perspective view of the distal end-portion in Fig. 3, clearly illustrating the position and shape of the end plug in the first lumen;
- 30 Fig. 5 shows a perspective view of the square-ended terminal portion of the catheter tube, the distal end of the vascular catheter still not mounted thereupon, whereby the cross-sectional shape of the catheter tube is clearly visible;
- 35 Fig. 6 shows a schematic elevational cross-sectional view through the distal end-portion of the vascular catheter, said distal end-portion contacting the vascular wall of the blood vessel;

Fig. 7 shows a schematic, dimension-wise slightly exaggerated side view of a distal end-portion, wherein both the first and the second sections thereof exhibit a substantially straight conical shape, and

5 Fig. 8 finally shows a schematic, dimension-wise slightly exaggerated side view of a distal end-portion, wherein both the first and the second sections thereof exhibit a substantially rounded conical shape.

10 DESCRIPTION OF EXEMPLARY EMBODIMENTS

In fig. 1, reference numeral 1 denotes a multilumen vascular catheter for treatment of, for example, dialysis patients. The vascular catheter 1 exhibits a proximal connection portion 10 for connection to, for example, a dialysis medical device (not shown), and a distal end-portion 12 adapted for insertion into a venous blood vessel 14. The blood vessel 14 is not shown in Fig. 1, but is later shown in Figs. 2 and 6, respectively.

20 A flexible catheter tube 16 is arranged between the proximal connection portion 10 and the distal end-portion 12. As shown in Fig. 2, the catheter tube 16 comprises a first lumen 18 for extraction of fluid such as for example untreated blood from the blood vessel 14, which is schematically shown in the figure. Further, the catheter tube 16 comprises a second lumen 20 for introducing fluid such as for example treated blood back to the blood vessel 14,

25 With reference back to Fig. 1, the vascular catheter 1 is provided – in a known manner – with extension tubes 13 connected to the respective lumen 18, 20 in the catheter tube 16. The extension tubes 13 are in turn provided with sealable valves 15 and are terminated with connection plugs 17. The extension tubes 13 are joined side-by-side to the catheter tube 16 via a Y-coupling 19. Additionally, fastening flanges 21 are attached to the Y-coupling 19 for temporary fixation on the skin of the patient, for example by means of adhesive tape (not shown) or by other means.

35 One or more suction openings 22 communicate with said first lumen 18. In the shown embodiment, there are four suction openings 22 (as shown in Fig. 3), which are located upstream of one or more outlet openings 24, which in turn communicate with said second lumen 20. Both the suction openings 22 and outlet openings 24 are located at said distal end-portion 12, which according to the invention is permanently

bulbous, offering a range of advantages. These advantages will be explained as the description unfolds below. In the embodiment shown in the drawings, the distal end-portion 12 is formed as a separate part, which is welded or glued to the catheter tube 16 upon assembly.

5

In Fig. 2, the flow direction is illustrated with the flow indication arrows 23. All references below as to the terms "upstream" and "downstream" are thus given with reference to this flow direction, which thus runs from left to right in Fig. 2.

10 As shown in Fig. 2, bulbous distal end-portion 12 is terminated with in a guide-wire opening 26 for a guide-wire 28 of a previously known, so called Seldinger-type, shown with phantom lines in Fig. 2. The guide-wire 28 is operated in the following known manner: A hollow syringe (not shown) is first used to puncture the blood vessel 14, whereafter the flexible guide-wire is inserted through the syringe and is
15 then pushed further into the blood vessel to a desired position. The syringe is then removed and the vascular catheter 1 is slid over the guide-wire 28 in the second lumen 20 and further to a desired position within the blood vessel 14 of the patient. The guide-wire 28 is then retracted from the blood vessel 14. The positioning of the catheter 1 in the blood vessel 14 is often carefully supervised in a known manner by
20 use of Ultrasound technology or other means.

As further illustrated in Fig. 2, the distal end-portion 12 exhibits a first, widening section A starting from the catheter tube 16 with a gradually increasing external cross-section in the direction towards said guide-wire opening 26. This first section A
25 transits downstream via a shoulder 30 with a maximum external diameter into a second, narrowing section B having a gradually decreasing external cross-section in the direction towards the guide-wire opening 26.

The suction openings 22 are located in the first, widening section A of the distal end-portion 12, whilst the outlet openings 24 are located in the second, narrowing section B of the distal end-portion 12.
30

The purpose of the bulbous distal end-portion 12 is primarily to achieve an increase in flow speed of the blood past the shoulder 30 with the maximum cross-sectional dimension, whereby undesired recirculation of treated blood back, i.e. against the flow, to the suction openings 22, is prevented according to the invention. Simultaneously a pressure 4 is created at the shoulder 30, i.e. a locally lower pressure than the normal blood pressure in the blood vessel 14. Since the outlet
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openings 24 are preferably located close to or immediately adjacent to the shoulder 30, the pressure 4 around the shoulder 30 facilitates the reunion of the treated blood from the outlet openings 24 to the blood vessel 14, as the returning blood through the second lumen 20 of the vascular catheter 1 has a higher relative pressure than
5 said locally lower pressure around the shoulder 30.

The maximum diameter of the bulbous end-portion 12 is calculated in such a way, that the cross-sectional area which remains in the blood vessel 14 around the shoulder 30, corresponds to "normal" vascular flow minus the flow which is to be
10 treated (below referred to as treatment flow". Thus, at a normal vascular flow of 15 l/min (which is a common normal vascular flow, varying somewhat depending on the individual) and at a desired treatment flow of 0,5 l/min, the maximum diameter should be chosen so that the remaining cross-sectional area between the shoulder 30 and the vascular wall 31 of the blood vessel 14 corresponds to a flow around the
15 shoulder 30 of 1,0 l/min. At a desired treatment flow corresponding, for example to 0,6 l/min, the maximum diameter is chosen so as to achieve a flow around the shoulder of 0,9 l/min etc. The first example may, with reference to Fig. 2, described in such a way that a normal vascular flow of 1,5 l/min exists upstream of the distal end-portion 12 of the vascular catheter 1, whereby a treatment flow corresponding
20 to 0,5 l/min is sucked into the suction openings 22 according to the flow indication arrows 25 when the blood passes by the suction openings 22. A remaining vascular flow corresponding to $1,5 \text{ l/min} - 0,5 \text{ l/min} = 1,0 \text{ l/min}$ is now forced under an increase in speed and a local pressure fall around the shoulder 30 of the bulbous distal end-portion 12, whereafter a treated flow corresponding to 0,5 l/min is
25 reintroduced into the remaining vascular flow via the outlet openings 24 according to the flow indication arrows 27, and, in the shown example, also through the guide-wire opening 26 according to the flow indication arrow 29. Downstream of the outlet openings 24 and the guide-wire opening 26, a normal vascular flow corresponding to 1,5 l/min is again occurring.

30

Both the first, widening section A and the second, narrowing section B of the distal end-portion 12 exhibit in Fig. 2, a rounded conical shape (in the shown example, primarily in vicinity in the shoulder 30) in such a way that the shoulder 30 forms a rounded transition between the two sections A, B.

35

In Fig. 2, it is also shown that the suction openings 22 are located adjacent to a narrow end 32 of the first, widening section A of the distal end-portion 12, at one or

more axial distances A_1 , A_2 from said narrow end 32 corresponding to between 5-20% of the length of the first, widening section A.

5 Furthermore, the outlet openings 24 are located adjacent to the shoulder 30 – as described above – at an axial distance b from said shoulder 30 corresponding to between 5-20% of the length of the second, narrowing section B. Preferably, the axial distance b corresponds to 5-10% of the length of the second, narrowing section B. The shoulder 30 preferably has an external cross-section (here *diameter*, since the distal end-portion 12 normally has a circular cross-section as shown in this case)
10 which exceeds the diameter of the catheter tube 16 by 10-20%.

The first, widening section A of the distal end-portion 12, in its internal periphery, exhibits an internal cylindrical recess 34 shaped to receive a corresponding end-portion 36 of the catheter tube 16. The internal cylindrical recess 34 is limited in the
15 axial direction of the widening section A, by a radial abutment edge adapted for abutment against a square-ended terminal end 40 of the end-portion 36 of the catheter tube 16.

The distal end-portion 12, downstream of the internal cylindrical recess 34, exhibits a
20 cylindrical bore 42, the internal diameter of which corresponds to the internal diameter of the catheter tube 16. The bore 42 is clearly visible in Fig. 2 and Fig. 4, and extends continually from the first, widening section A into the second, narrowing section B of said distal end-portion 12.

25 Furthermore, an end plug 44 is inserted into said first lumen 18 at the square-ended terminal end 40 of the end-portion 36 of the catheter tube 16. The end plug 44 is arranged to prevent communication between said first lumen 18 and said second lumen 20. According to the invention, the end plug 44 exhibits an abutment surface 46 for abutment against said square-ended terminal end 40 of the end-portion of the
30 catheter tube 16, a portion 48 of the end plug 44 extending upstream from said abutment surface 46 into said first lumen 18 to a suction opening 22. The end plug 44 extends downstream into said cylindrical bore 42, and further on to – or just upstream of – one of said outlet openings 24.

35 A multilumen vascular catheter (1) according to claims 10 or 11, characterized in that said end plug (44) exhibits a first upstream, doubly arced and upstreamingly slanted end surface (50) forming a smooth transition between said first lumen (18) and at least one of said suction openings (22).

The end plug 44 exhibits a first downstream, doubly arced and upstreamingly slanted end surface 50 forming a smooth transition between said second lumen 18 and at least one of said suction openings 22. Furthermore, the end plug 44 exhibits a first
5 downstream doubly arced and downstreamingly slanted end surface 52 forming a smooth transition between said second lumen 20 and at least one of said outlet openings 24. The smooth transitions prevent build up of flow restricting blood coagulations, that may otherwise form at the suction openings 22 or the outlet openings 24, particularly when the vascular catheter 1 is inserted into the blood
10 vessel 14 under a longer period of time.

A favourable method for production of a vascular catheter according to the invention, is characterized in that the end plug 44 is first mounted in said first lumen 18 in such a way that its abutment surface 46 abuts the square-ended terminal end 40 of the
15 end-portion 36 of the catheter tube 16. Then the distal end-portion 12 is mounted on the end-portion 36 of the catheter tube 16, said mounting of said parts being effected by welding and/or by gluing. When welding is used, the parts are suitably welded together in a single welding step.

20 For the sake or clarity, Fig. 3 shows an "X-ray"-perspective view of the distal end-portion 12 of the vascular catheter 1. In the shown embodiment, four substantially circular suction openings 22 are located in two rows at a mutual distance from each other. The suction openings 22 are hereby shown with phantom lines. Furthermore, four substantially circular outlet openings 24 are equally distributed around the
25 second, narrowing section B of the distal end-portion 12, immediately downstream of the shoulder 30.

In Fig. 4, a cross-sectional perspective view of the distal end-portion 12 in Fig. 3 is shown, clearly illustrating the position and shape of the end plug 44 in the first
30 lumen 18. Here, the shape of the two slanted doubly arced end-surfaces 50 and 52, respectively are also shown.

Fig. 5 shows a perspective view of the end-portion 36 of the catheter pipe 16 when the distal end-portion 12 is not yet mounted onto the catheter tube 16. The cross-
35 sectional shape of the catheter tube 16 is also shown in the figure. The first lumen 18 is separate from the second lumen 20 by means of a partition wall 37. The partition wall 37 extends along the entire length of the catheter tube 16 and is arced and mounted in the catheter tube 16 in such a way that the cross-sectional areas are

substantially equal. In one embodiment of the invention, the cross-sectional area of the first lumen 18 – which lumen communicates with the suction openings 22 – slightly exceeds the corresponding cross-sectional area of the second lumen 20, which communicates with the outlet openings 24. The reason for this difference in cross-sectional area is that the so called wet area for the first lumen 18 is slightly larger than that of the second lumen 20, which means that a larger pressure fall is created in said first lumen 18. In order to compensate for the relatively higher pressure fall, the cross-sectional area should thus be slightly larger than that of the first lumen 18, in order to obtain equal pressure losses in both lumina 18, 20. The difference in cross-sectional area is, however, relatively small, which may be illustrated in an example with a vascular catheter 1 of the dimension 14 French, which corresponds to a diameter of the catheter pipe 16 of 5,7 mm. The cross-sectional area for the first lumen is then, according to a favourable embodiment, 7,00 mm², whilst the cross-sectional area for the second lumen 20 is 5,19 mm². Together, they form a “wet” cross-sectional area of 12,19 mm², which by means of the shown cross-sectional shape and the thereby enabled thinner wall dimensions, is larger than what is known today in 14 French catheters, which normally do not have a larger total wet cross-sectional area than 10,8 mm². The design of the special cross-sectional shape of the catheter tube 16 also means that deformations in the partition walls 37 as a result of the blood pressure in lumen 18, 20, respectively are prevented to a large extent. The partition wall 37 further exhibits rounded abutment portions at the transitions to the remaining part of the catheter tube 16 in order to avoid blood coagulation build-up.

In Fig. 5, the suction openings 22 are also shown located in the end-portion 36 of the catheter tube 16.

Fig. 6 shows a schematic elevational cross-sectional view through the distal end-portion 12 of the vascular catheter 1, said distal end-portion 12 contacting the vascular wall 31 of the blood vessel. This illustrates a common situation in which a vascular catheter in reality seldom lies centered in the blood vessel 14 in the way shown in Fig. 2. The design of the bulbous distal end-portion 12 according to the invention, ensures that one or several of the suction openings 22 are not sucked into direct abutment against the vascular wall 31 of the blood vessel 14. In this situation, the distal end-portion 12 abuts the vascular wall 31 of the blood vessel 14 with its shoulder 30.

Fig. 7 shows a schematic, dimension-wise slightly exaggerated side-view of a distal end-portion 12, wherein both the first, widening section A and the second, narrowing section B of the end-portion 12 exhibit a substantially straight conical shape. However, an axially limited round-off is located at the shoulder 30.

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Fig. 8 finally shows a schematic, dimension-wise slightly exaggerated side-view of a distal end-portion, wherein both the first, widening section A and the second, narrowing section B over the end-portion 12 exhibits a substantially continuously rounded conical shape.

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The invention is not limited to the embodiments shown in the drawings and described above, but may be varied freely within the scope of the appended claims. For example, the catheter tube 16 may be provided with a central, separately formed, third lumen (not shown) arranged for the guide-wire 28 and eventual subsequent intravenous supply of medical substances. The catheter tube 16, as well as its distal end-portion 12 may be made of a number of alternative materials, that are used in a known manner in the manufacture of multilumen catheters 1. Such materials include, for example, different silicone materials or thermoplastics such as polyvinylchloride (PVC), polyurethane, polyamide, polyethylene or polypropene. Preferably, however, polyurethane or polyurethane based materials are used, such as for example Carbothane® as a material for the catheter tube 16.

15

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LIST OF REFERENCE NUMERALS

1. Vascular catheter
10. Proximal connection portion
- 5 12. Distal connection portion
13. Extension tube
14. Blood vessel
15. Sealable valves
16. Catheter tube
- 10 17. Connection plugs
18. First lumen
19. Y-coupling
20. Second lumen
21. Fastening flanges
- 15 22. Suction openings
23. Flow indication arrows
24. Outlet openings
25. Flow indication arrows for untreated blood flowing into the suction openings
- 20 26. Guide-Wire opening
27. Flow indication arrows for treated blood flowing out of the outlet openings
28. Guide-wire
29. Flow indication arrow for treated blood flowing out of the guide-wire opening
- 25 30. Shoulder
31. Vascular wall of blood vessel
32. Narrow end of the first, widening section A
34. Internal cylindrical recess
- 30 36. End-portion of catheter tube
37. Partition wall
38. Radial abutment edge
39. Rounded abutment portions
40. Square terminal end of catheter tube
- 35 42. Cylindrical bore
44. End plug
46. Abutment surface of end plug
48. Inserted portion of end plug (into first lumen)

- 50. First slanted end surface of end plug
- 52. Second slanted end surface of end plug

- A: First, widening section of distal end portion
- 5 B: Second, narrowing section of the distal end portion
- a₁: Axial distance for suction opening
- a₂: Axial distance for suction opening
- b: Axial distance for outlet opening

CLAIMS:

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1. A multilumen vascular catheter (1) for treatment of patients by insertion of said vascular catheter (1) in a venous blood vessel (14) by means of a guide-wire (28), said vascular catheter (1) comprising:

- a proximal connection portion (10);
- 10 - a distal end-portion (12) which is terminated with in a guide-wire opening (26);
- a flexible catheter tube (16) arranged between the proximal connection portion (10) and the distal end-portion (12), said catheter tube (16) comprising a first lumen (18) for extraction of fluid such as for example untreated blood from the vessel (1) and a second lumen (20) for introducing fluid such as for example treated blood to
- 15 the blood vessel (14);

- one or more suction openings (22) communicating with said first lumen (18), said suction openings (22) being located upstream of one or more outlet openings (24), which in turn communicate with said second lumen (20), said suction openings (22) and outlet openings (24) being located at said distal end-portion (12),

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characterized in:

- that the distal end-portion (12) is permanently bulbous and exhibits a first, widening section (A) starting from the catheter tube (16) with a gradually increasing external cross-section in the direction towards said guide-wire opening (26), said first section (A) transiting downstream via a shoulder (30) with a maximum external
- 25 diameter into a second, narrowing section (B) having a gradually decreasing external cross-section in the direction towards the guide-wire opening (26), and
- that said one or more suction openings (22) are located in the first, widening section (A) of said distal end-portion (12), whilst said one or more outlet openings (24) are located in the second, narrowing section (B) of said distal end-portion (12).

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2. A multilumen vascular catheter (1) according to claim 1, **characterized in** that said first, widening section (A) of said distal end-portion (12) exhibits a substantially conical shape.

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3. A multilumen vascular catheter (1) according to claim 1 or 2, **characterized in** that said second, narrowing section (B) of said distal end-portion (12) exhibits a substantially conical shape.

4. A multilumen vascular catheter (1) according to claims 2 and 3, **characterized in** that both the first, widening section (A) and the second, narrowing section (B) of said distal end-portion (12) exhibit a rounded conical shape, in such a way that the shoulder (30) forms a rounded transition between the two sections (A, B).
- 5
5. A multilumen vascular catheter (1) according to any of the preceding claims, **characterized in** that said one or more outlet openings (24) are located adjacent to the shoulder (30), at an axial distance (b) from said shoulder (30) corresponding to between 5-20% of the length of the second, narrowing section (B).
- 10
6. A multilumen vascular catheter (1) according to any of the preceding claims, **characterized in** that said one or more suction openings (22) are located adjacent to a narrow end (32) of the first, widening section (A) of the distal end-portion (12), at one or more axial distances (a_1 , a_2) from said narrow end (32) corresponding to
- 15
- between 5-20% of the length of the first, widening section (A).
7. A multilumen vascular catheter (1) according to any of the preceding claims, **characterized in** that said shoulder (30) has an external cross-section exceeding the diameter of the catheter tube (16) by 10-20%.
- 20
8. A multilumen vascular catheter (1) according to any of the preceding claims, **characterized in** that the first, widening section (A) of the distal end-portion (12), in its internal periphery, exhibits an internal cylindrical recess (34) shaped to receive a corresponding end-portion (36) of the catheter tube (16), said internal cylindrical
- 25
- recess (34) being limited in the axial direction of the widening section (A), by a radial abutment edge (38) adapted for abutment against a square-ended terminal end (40) of the end-portion (36) of the catheter tube (16).
9. A multilumen vascular catheter (1) according to claim 8, **characterized in** that
- 30
- the distal end-portion (12), downstream of the internal cylindrical recess (34), exhibits a cylindrical bore (42), the internal diameter of which corresponds to the internal diameter of the catheter tube (16), said bore (42) extending continually from the first, widening section (A) into the second, narrowing section (B) of said distal end-portion (12).
- 35
10. A multilumen vascular catheter (1) according to claim 9, wherein an end plug (44) is inserted into said first lumen (18) at the square-ended terminal end (40) of the end-portion (36) of the catheter tube (16), said end plug (44) being arranged to

prevent communication between said first lumen (18) and said second lumen (20),
characterized in that the end plug (44) exhibits an abutment surface (46) for
abutment against said square-ended terminal end (40) of the end-portion (36) of the
catheter tube (16), a portion (48) of the end plug (44) extending upstream from said
5 abutment surface (46) into said first lumen (18) to a suction opening (22).

11. A multilumen vascular catheter (1) according to claim 10, **characterized in** that
said end plug (44) extends downstream into said cylindrical bore (42), and further on
to – or just upstream of – one of said outlet openings (24).

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12. A multilumen vascular catheter (1) according to claims 10 or 11, **characterized
in** that said end plug (44) exhibits a first upstream, doubly arced and upstreamingly
slanted end surface (50) forming a smooth transition between said first lumen (18)
and at least one of said suction openings (22).

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13. A multilumen vascular catheter (1) according to any of claims 10-12,
characterized in that said end plug (44) exhibits a first downstream, doubly arced
and downstreamingly slanted end surface (52) forming a smooth transition between
said second lumen (20) and at least one of said outlet openings (24).

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14. Method for producing a multilumen vascular catheter (1) according to claims 10-
13, **characterized in** that the end plug (44) is first mounted in said first lumen (18)
in such a way that its abutment surface (46) abuts the square-ended terminal end
(40) of the end-portion (36) of the catheter tube (16), whereafter the distal end-
25 portion (12) is mounted on the end-portion (36) of the catheter tube (16), said
mounting of said parts being effected by welding and/or by gluing.

15. Method according to claim 14, **characterized in** that said parts are welded
together in a single welding step.

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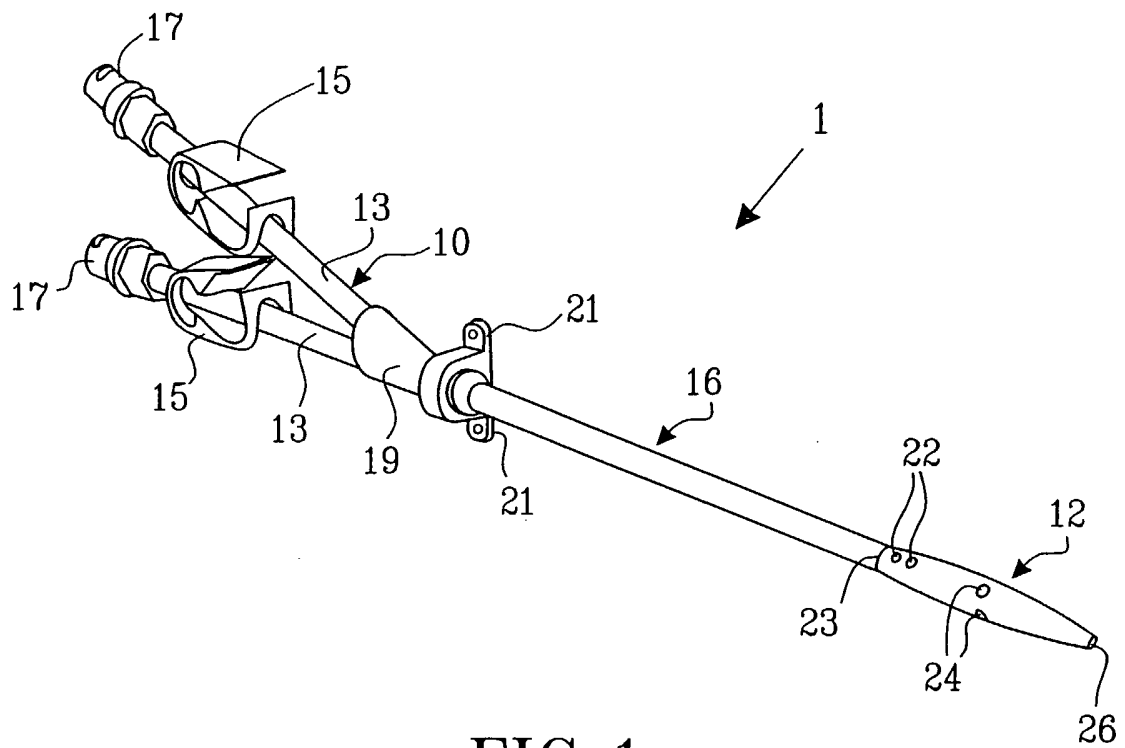


FIG. 1

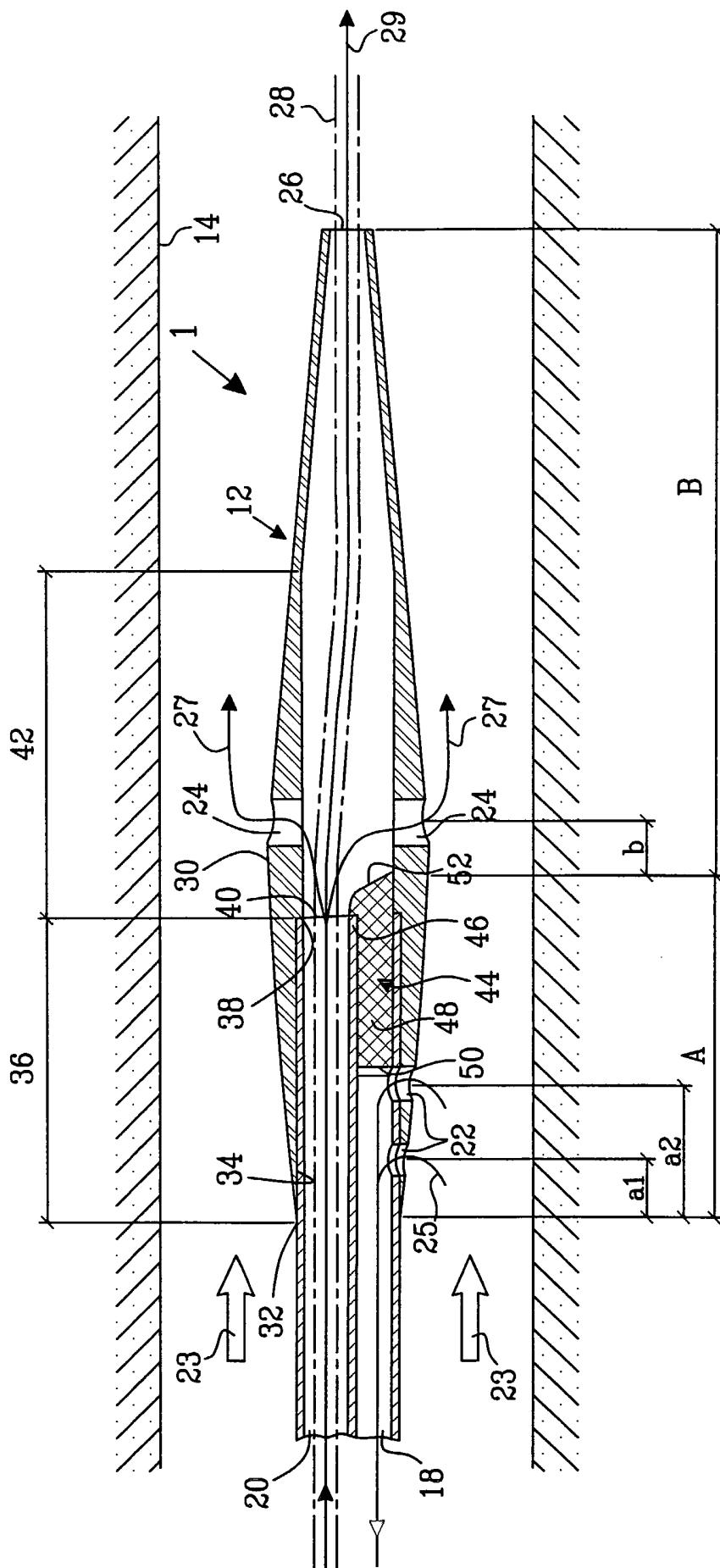


FIG.2

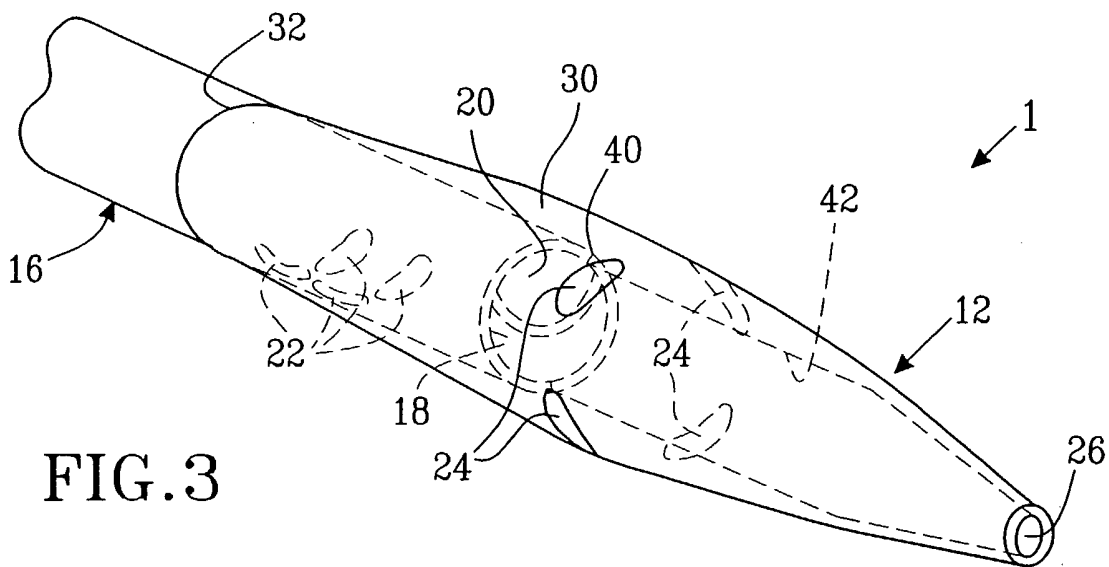


FIG. 3

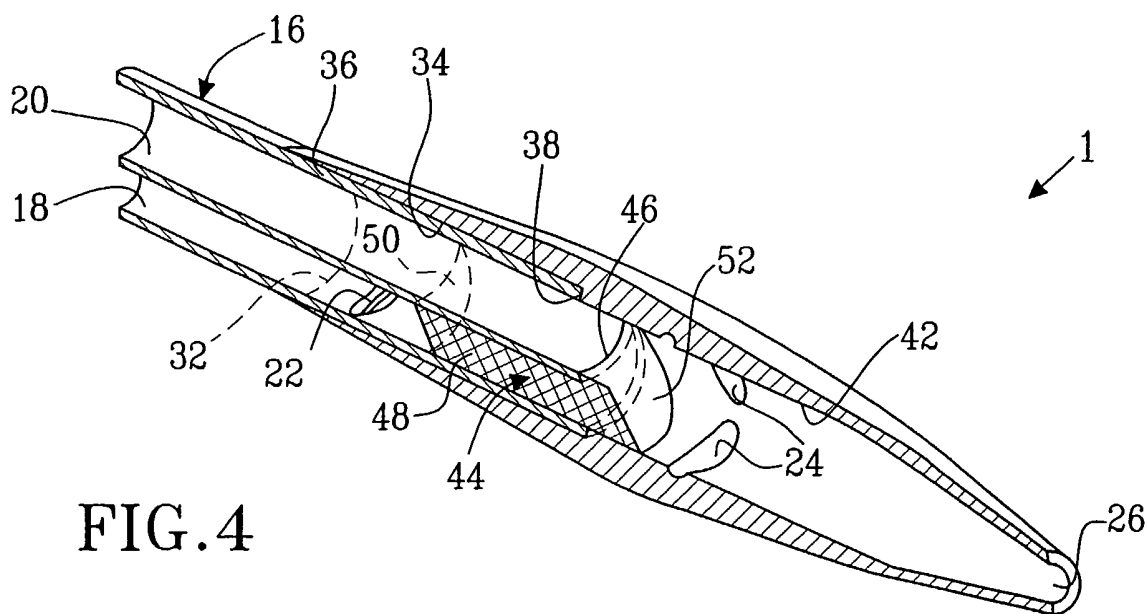


FIG. 4

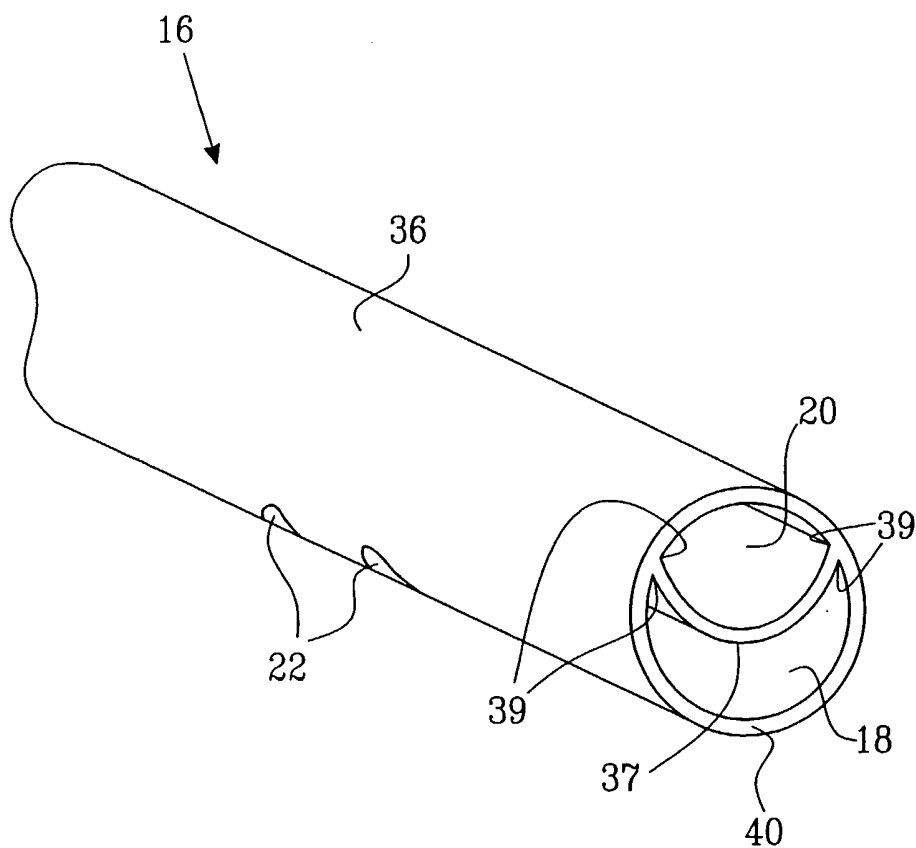


FIG.5

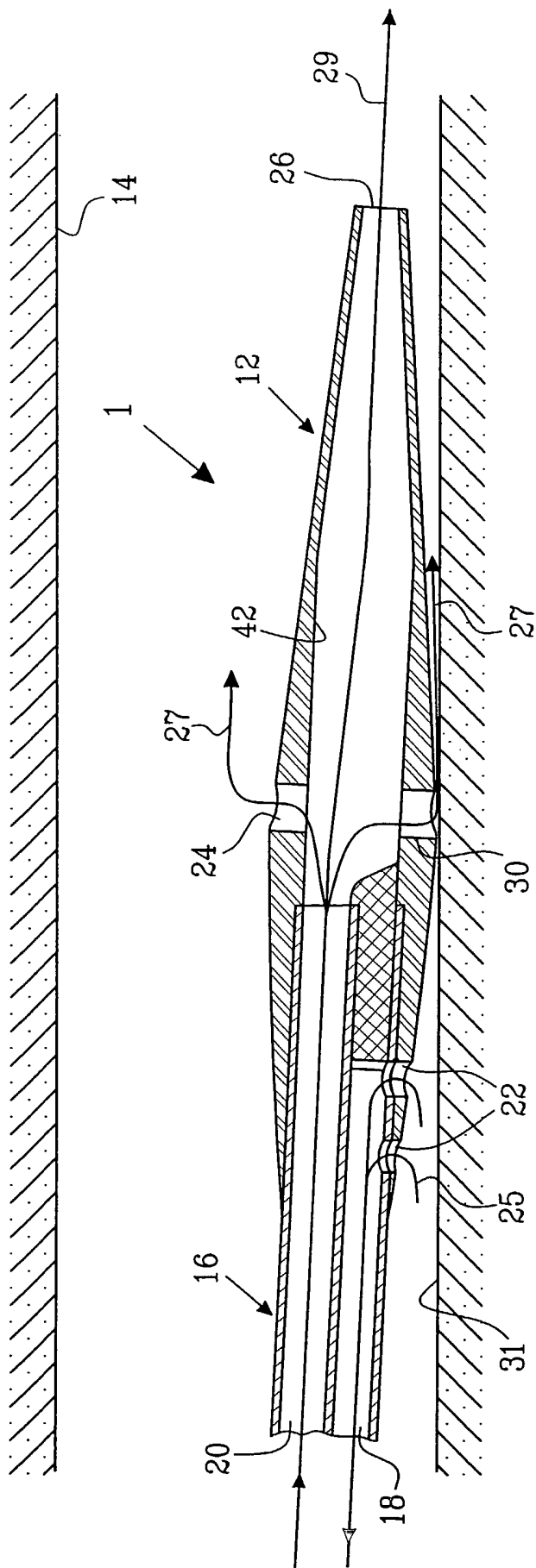


FIG. 6

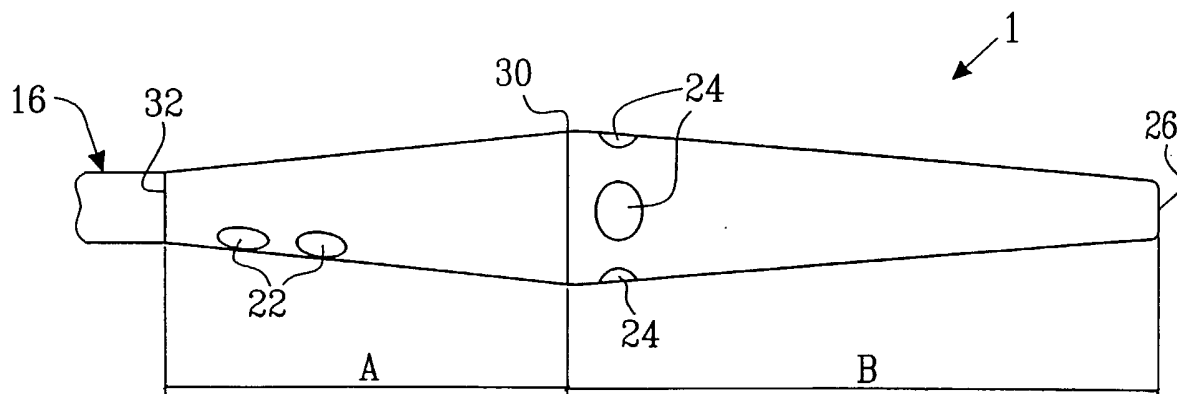


FIG. 7

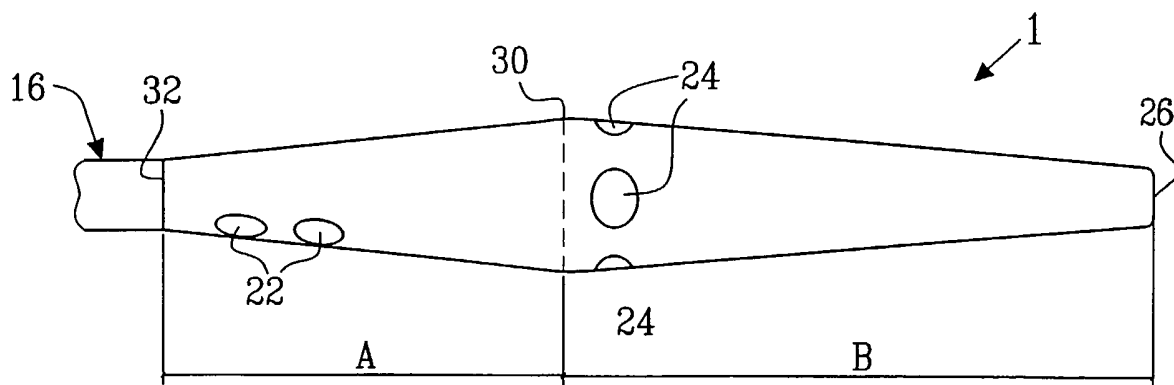


FIG. 8

INTERNATIONAL SEARCH REPORT

International application No.

PCT/SE 2004/000621

A. CLASSIFICATION OF SUBJECT MATTER

IPC7: A61M 25/00, A61M 25/14, A61M 25/16

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC7: A61M

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

SE,DK,FI,NO classes as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-INTERNAL, WPI DATA, PAJ

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 6206849 B1 (GEOFFREY S. MARTIN ET AL), 27 March 2001 (27.03.2001), The whole document --	1-15
A	US 5009636 A (RONALD W. WORTLEY ET AL), 23 April 1991 (23.04.1991), The whole document --	1-15
A	US 4894057 A (RANDOLPH M. HOWES), 16 January 1990 (16.01.1990), The whole document --	1-15
A	EP 0299622 A2 (MINNESOTA MINING AND MANUFACTURING COMPANY), 18 January 1989 (18.01.1989), The whole document --	1-15

 Further documents are listed in the continuation of Box C. See patent family annex.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

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"X" document of particular relevance: the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance: the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

14 June 2004

Date of mailing of the international search report

13 -07- 2004

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INTERNATIONAL SEARCH REPORT

International application No.
PCT/SE 2004/000621

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
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