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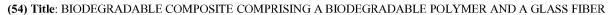
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(57) Abstract: The invention is directed to biodegradable composite comprising a biodegradable polymer and 20-70 vol% glass fibers, wherein the biodegradable composite has a flexural strength between 100 and 600 MPa and to a process for the preparation of a biodegradable composite comprising a biodegradable polymer and a glass fiber, wherein a the glass fibers are pre-treated with a solution of the biodegradable polymer in a solvent; b. the solvent is evaporated; c. the pre-treated glass fibers, optionally together with additional biodegradable polymer, is placed in a mold, where after the biodegradable polymer present on the glass fibers and/or added to the mold is melted by applying heat and pressure; d. the mold is cooled and the biodegradable composite is removed from the mold.

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BIODEGRADABLE COMPOSITE COMPRISING A BIODEGRADABLE POLYMER AND A GLASS FIBER

The invention is directed to a biodegradable composite comprising a biodegradable polymer and 20-70 vol% glass fibers, a process for the preparation of a biodegradable composite and a medical implant comprising a biodegradable composite.

In orthopedic applications that require high strength, usually stainless steel or titanium alloys are used. Although these materials are inert, they are also used in situations in which the need for the implant is only temporary, like in fracture fixation. Often the implant has to be retrieved during a second surgery after healing because of inflammation of the host tissue. Besides that, stress shielding can occur due to the high stiffness of the metals, so that bone loses its original strength. Other disadvantages are that the metal implants are palpable and a cold sensation can occur.

In addition to the conventional metal devices, several polymer devices for temporary orthopedic applications were developed, that can be broken down by the human body. No second surgery to retrieve the implant is needed, but the strength of these devices is still insufficient.

This drawback can potentially be overcome by using composite technology. In composite materials, usually a relatively flexible matrix is combined with a stiff and strong reinforcement material to enhance the mechanical properties of the matrix. For these temporary high-strength applications, biodegradable glass or mineral material can be used to improve the stiffness and strength of a biodegradable polymer matrix. In the prior art several attempts to produce such a composite were reported. According to the prior art bioactive glass particles, hydroxyapatite powder, or short glass fibers were used to enhance the properties of a biodegradable polymer.

At the moment no appropriate biodegradable material is available for fraction fixation or other load-bearing orthopedic applications, because of the high strength that is required for this composite material.

However, the fracture strength of these composites is still low.

There thus is a need for a composite material which is biodegradable and that can be used in medical applications that require high strength and a stiffness compared to the stiffness of bone. These medical applications include fracture fixation, tendon reattachment, spinal fixation, and spinal cages.

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It has now surprisingly been discovered that a biodegradable composite material can be prepared from a biodegradable polymer and 20-70 vol% glassfibers, wherein the biodegradable composite has a flexural strength between 100 and 600 MPa. Preferably, the biodegradable composite has a flexural strength between 150 and 500 MPa; more preferably between 250 and 500 MPa.

Preferably, the biodegradable composite also has a flexural modulus between 10 and 40 GPa, preferably between 15 and 35 GPa; more preferably between 20 and 35 GPa.

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In the biodegradable composite material according to the invention 20-70 vol% of glass fibers is used. Preferably, 30-60 vol%, more preferably 40-55 vol% glass fibers is used in the composite. The glass fibers that can be used are long (with an average length of more than 1.5 mm) or continuous fibers.

The glass fibers can be used in the biodegradable composite in a number of forms, such as strands, bundles, filaments, yarn, mats, woven fabrics and unwoven fabrics or roving. A continuous fiber can also be formed into a structure by using filament winding. Composites containing continuous fibers have a higher flexural strength than composites comprising long glass fibers. Composites containing continuous fibers are therefore preferred. The glass fibers can contain various sizings and finishes. A sizing is a surface treatment or coating applied to the glass fibers during the forming operation. A finishing is a surface treatment applied to the glass fibers after heat cleaning. This treatment usually consists of a water- or solvent-diluted coupling agent, which are designed to provide good interfacial adhesion of glass to the polymer.

Preferably, the biodegradable composite comprises glass fibers having a SiO₂ content of 15-60 wt%; preferably 20-50 wt%; more preferably 20-40 wt%.

Most preferably, the glass fibers are resorbable glass fibers. Resorbable means that the glass fibers are resorbed in the human or animal body mainly under the influence of water and/or enzymes. Resorbable glass fibers not always contain SiO_2 , but these glass fibers preferably contain more than 0.5 wt% of P_2O_5 .

Specific examples of glass fibers that can be used are resorbable glass fibers of Vivoxid and Giltech.

The biodegradable composite also comprises a biodegradable polymer. A biodegradable polymer is a polymer that can decompose in the human or animal body during a certain period of time. Decomposition of the biodegradable polymer occurs mainly under the influence of water and/or enzymes.

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used.

Examples of biodegradable polymers are $poly(\alpha\text{-esters})$, which include poly(lactic acid), poly(glycolic acid), poly(p-dioxanone) and poly(3-hydroxybutyrate); tyrosine-derived polymers, which include polycarbonates, polyarylates and copolymers of these with polyethyleneglycol (PEG); natural polymers, which include starch, chitosan, collagen, cellulose, including methyl cellulose and chitin; $poly(\epsilon\text{-caprolactone})$, poly(propylene fumarate) and poly(trimethylene carbonate). It is also possible to use (block)copolymers made from the various monomers used to prepare the biodegradable polymers mentioned above.

Mixtures of the above-mentioned biodegradable polymers can also be

The poly(α -esters), more preferably poly(lactic acid), are preferred because the mechanical properties, i.e. the stiffness and strength, of these polymers are sufficient for use in a composite material.

The invention is also directed to a process for the preparation of a biodegradable composite, wherein

- a. the glass fibers are pre-treated with a solution of the biodegradable polymer in a solvent;
- b. the solvent is evaporated;
- c. the pre-treated glass fibers, optionally together with additional biodegradable polymer, is placed in a mold, where after the biodegradable polymer present on the fibers and/or added to the mold is melted by applying heat and pressure;
- d. the mold is cooled and the biodegradable composite is removed from the mold.

The solution of the biodegradable polymer can be easily made by the person skilled in the art. For instance, the solution can be made by dissolving granules of the biodegradable polymer in a suitable solvent. A dispersion of very small (i.e. submicron) polymer particles in a liquid can act as a solution, and thus can be used as well.

Examples of suitable solvents are water, alcohols, acetone, ethyl acetate, butanone, dimethyl sulfoxide, 1, 4-dioxane, tetrahydrofurane and chloroform.

The concentration of the biodegradable polymer in the solvent can be chosen within wide ranges and depends, for instance, on the amount of biodegradable polymer that one wants to apply on the fiber-containing glass fiber.

Evaporation of the solvent can be performed faster by the application of heat or an air stream.

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The pre-treated glass fiber is placed in a mold, where after the biodegradable polymer present on the filer is melted by applying heat and pressure. In this way a composite is made and a good contact between the glass fiber and the biodegradable polymer is obtained.

It is possible to apply all biodegradable polymer onto the glass fiber by repeating the application of the solution of the biodegradable polymer on the glass fiber and evaporating the solvent several times. In this way one is able to apply more biodegradable polymer onto the glass fiber, but applying the solution and drying is time consuming. Thus, normally application of just one layer is performed to obtain a good contact between the glass fiber and the biodegradable polymer.

The rest of the biodegradable polymer in the composite is applied to the mold together with the pre-treated glass fiber. The biodegradable polymer can be mixed with the pre-treated glass fiber, or applied to the mold before, after or between the pre-treated glass fibers.

After filling the mold is closed and the biodegradable polymer is melted in the mold by applying heat and pressure.

The best adhesion between the glass fiber and the biodegradable polymer is obtained when the biodegradable polymer used for the pretreatment of the glass fiber is the same as the biodegradable polymer added to the mold. The better the adhesion between the glass fiber and the biodegradable polymer is, the better are the stiffness and the strength of the composite.

The composite according to the invention may further contain one or more additives such as stabilizers, anti-oxidants, colorants, fillers, binders, fibers, meshes, substances providing radio-opacity, surface active or surface modifying agents, foaming agents, processing aids, plasticizers, biostatic/biocidal agents, substances that provide or trigger bioactivity and any other known agents.

Suitable examples of other fillers, which can be used in the composite in a small amount (for instance not more than 1 wt%), are e.g. bone-mineral based fillers, and binders which are described in U.S. Patent Number 6,808,585B2 in columns 8-10 and in U.S. Patent Number 7,044,972B2 in column 4, I. 30-43, which are herein incorporated by reference. Typical fillers are selected from the group of calcium-based fillers (such as calcium phosphate, hydroxyapatite, tricalcium phosphate, calcium sulfate, demineralized bone, autologous bone, coralline substances).

The invention is also directed to a medical implant comprising the biodegradable composite.

Examples of medical implants are a screw, a pin, a plate, a suture, a mesh, a net, a film, a tube, a balloon, a bag, a rod, an anchor, a valve, a ring, a stent, a cage, a spacer, a graft, a porous or open structure, a scaffold and/or components thereof.

The invention will hereafter be described in more detail by the following examples that by no means limit the scope of the invention.

EXAMPLES

10 Materials

Biodegradable polymers:

Poly(lactic acid) (PLA): 4032D from Natureworks LLC

Methyl cellulose (MC): Methyl from Perfax

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Solvent

Chloroform: solvent obtained from Sigma-Aldrich

Glass fibers

- Glass fiber textile: Satin weave SS0303 from Ten Cate Advanced Composites Chemical composition: 52-56 wt% SiO2, 16-25 wt% CaO, 12-16 wt% Al2O3, 5-10 wt% B2O3, 0-2 wt% NaO and K2O, 0-5 wt% MgO, 0.05-0.4 wt% Fe2O3, 0-0.8 wt% TiO2, 0-1.0 wt% fluorides
- Continuous glass fiber: EC9 136 from PPG
 Chemical composition: 52-56 wt% SiO2, 16-25 wt% CaO, 12-16 wt% Al2O3, 5-10 wt% B2O3, 0-2 wt% NaO and K2O, 0-5 wt% MgO, 0.05-0.4 wt% Fe2O3, 0-0.8 wt% TiO2, 0-1.0 wt% fluorides

Flexural test

The flexural modulus and flexural strength of the composites were determined according to ASTM test D790 on a Zwick/Roell 20 kN test bench. Test samples were prepared with a Unitom cutting machine while cooled with water to avoid defects on the edges that can cause premature failure. The flexural modulus was measured as the tangent at a loading of 20 N.

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The maximal flexural strength (oflex) is based on the maximal loading

(Fmax):

σflex = 3FmaxLspan

5 2wt²

with:

 $L = 40 \cdot tmean$

in which Lspan is the span length, w is the width of the specimen, t is the thickness of the specimen, and tmean is the average thickness of specimens of one composite.

<u>Imaging</u>

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Three imaging techniques were utilized to gain insight in the quality of the composite: optical microscopy, scanning electron microscopy (SEM), and ultrasonic transmission scanning (C-scanning). Cross sections and interlaminar sections of test specimens were investigated with optical microscopy and SEM, while complete plates were investigated with C-scanning.

The sections of test specimens were sometimes embedded and polished to optimize the quality of the resulting images.

Optical microscopy was performed on a Leica DC 300F microscope with which magnifications varying from 2.5 to 100 could be obtained. In an optical microscope, visual light and a system of lenses are used to image small samples. In depth imaging of samples is not possible with this technique and limited magnification is feasible. Optical microscopy was used to get an indication of the quality of the composites.

Scanning electron microscopy was executed on a JEOL-JSM7500F. SEM images sample surfaces by scanning with a high-energy beam of electrons and measuring the electrons that are scattered by the surface as well as the electrons produced by it. SEM is able to image samples in depth and to magnify from 25 up to 10⁶ times. With this imaging technique, the quality of the composite, including wetting of fibers, voids, microcracks, and adhesion was investigated, as well as the failure mechanism occurring in the flexural test.

Ultrasonic transmission scanning was performed on a Midas system. With this technique, the acoustic impedance of a material is measured by transmitting

ultrasonic energy to the sample and measuring the reflected energy. In a program (ALIS), the intensity of the reflected energy is converted from decibels to a tone of grey, in which darker grey represents a higher intensity.

The acoustic impedance is increased by voids, cracks, porosity, fibermatrix interfaces, fiber distribution, fiber volume fraction, foreign inclusions, and so on.
Consequently, dark grey indicated that more irregularities were present in that area.
Intact parts of the composite plates were scanned in order to make a rough estimation of the quality of the composite.

10 Sample preparation

Comparative experiment A

The steps that were carried out in the preparation of a composite of PLA sheets and glass fiber textile are listed below.

- 15 1. The PLA granules were dried in an oven at 80 °C during five hours.
 - 30 g PLA granules were compressed to sheets according to the protocol given below. This was repeated nine times to obtain nine sheets. The resulting sheets had a thickness of 1-2 mm.
 - 3. Eight sheets (30x30 cm) of glass fiber textile were made.
- 4. The eight glass fiber textiles and nine PLA sheets were subsequently stacked, and consolidated in a Joos press (LAP100) by heating up the stack while compression was applied. The protocol used in this process was a standard consolidation protocol of the Joos press.

25 Pressing protocol of PLA sheets

Heat up press to 200 °C.

Stack stainless steel plates, Teflon sheets (to separate the PLA from the press), and PLA granules.

Heat up PLA without applying pressure during 10 minutes

- 30 Apply 10 kN during 5 minutes
 - Apply 20 kN during 5 minutes
 - Apply 30 kN during 5 minutes
 - Apply 40 kN during 5 minutes
 - Apply 50 kN during 5 minutes
- 35 Apply 60 kN during 5 minutes

Remove Teflon sheets with PLA sheet in between from the press Cool the PLA sheet in ambient air during approximately 5 minutes Separate PLA sheet from Teflon sheets

5 Comparative experiment B

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The steps that were carried out in the preparation of a composite of glass fiber textile and PLA powder are listed below.

- 1. The mass of the PLA and the number of glass fiber textiles was calculated based on the required dimensions and fiber volume fraction. The goal was to make a plate of 300x150x2.5 mm with a fiber volume fraction of 0.5. To obtain this, nine sheets of glass fiber textile were needed, combined with 80 g of PLA.
- 2. The PLA granules were ground three times in a concentric grinder under nitrogen to granules with a diameter of approximately 1-2 mm.
- 15 3. Eight sheets (30x15 cm) of glass fiber textile were made.
 - 4. 8 g of PLA powder was distributed manually over the bottom of the mold. After this a glass fiber textile sheet was added on top of this layer. Then the next 8 g of PLA was distributed on top of the glass fiber textile. This was repeated until nine layers of PLA and eight layers of glass fiber textile were stacked subsequently. Finally, the mold was closed.

The system was consolidated in a Fontijne press (TP 1000). The consolidation steps are shown below.

Consolidation protocol of the composite of glass fiber textiles and PLA powder.

25 Heat up press to 200 °C.

Place the mold in the press and use Teflon sheets to separate the mold from the press Apply a force of 5 kN during 13 minutes

Apply a force of 8 kN during 9 minutes

Cool down the press to 41 °C, while the applied force is maintained at 8 kN

Take the mold out of the press and open it

Example I

The steps that were carried out in the preparation of a composite of pre-wetted glass fiber textiles are listed below.

- The mass of PLA and the number of glass fiber textiles was calculated based on the required dimensions. The goal was to make a plate of 300x150x2.5 mm. Therefore, eleven sheets of glass fiber textiles were combined with 73 g PLA.
- 5 2. Eleven sheets (30x15 cm) of glass fiber textile were made.
 - A solution of PLA and chloroform was prepared by adding
 g PLA granules in parts to 800 mL chloroform. The solution was stirred overnight.
 - 4. Multiple layers of the solution were applied to eleven glass fiber textiles (30x15 cm). The first layer was applied by dipping the sheets in the solution, while the following layers were applied to the sheets with a brush. Before a next layer was added, the sheets were dried for at least one hour in a hood on a Teflon sheet.
 - 5. The textiles were cut into rectangular impregnated textiles of 14x29 cm.
- 15 6. The eleven sheets were stacked on top of each other in the mold and the mold was closed. The composite was consolidated in a Fontijne press. The steps of the consolidation process are shown below. During the process, the temperatures in the mold were monitored.

20 <u>Consolidation protocol of prewetted glass fiber textiles.</u>

Heat up press to 200 °C.

Place the mold in the press and use Teflon sheets to separate the mold from the press Apply a force of 20 kN during 15 minutes

Apply a force of 30 kN during 4 minutes

25 Apply a force of 50 kN during two minutes

Cool down the press to 36 °C, while the applied force is maintained at 50 kN Take the mold out of the press and open it.

Example II

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- The steps that were carried out in the preparation of a composite of pre-wetted glass fiber textiles and PLA powder are listed below.
 - The mass of the PLA and the number of glass fiber textiles was calculated based on the required dimensions and fiber volume fraction. The goal was to make a plate with the same dimensions and fiber volume fraction as the plate

- obtained from glass fiber textiles combined with PLA powder. Therefore, eight sheets of glass fiber textile were needed and 80 g of PLA was added to this.
- 2. Eight sheets (30x15 cm) of glass fiber textile were made.
- 3. The PLA granules were ground three times in a concentric grinder under nitrogen to granules with a diameter of approximately 1 mm.
- 4. A solution of 11 g in 110 mL chloroform was prepared. The solution was applied to one side of the glass fiber textiles with a brush.
- 5. A solution of 11 g in 110 mL chloroform was prepared. The solution was applied to the other side of the glass fiber textiles with a brush.
- 6. 6 g of PLA powder was distributed manually over the bottom of the mold. After this, a glass fiber textile sheet was added on top of this layer. This was repeated until nine layers of PLA and eight layers of glass fiber textile were stacked subsequently. Finally, the mold was closed.
 - 7. The composite was consolidated in a Joos press, of which the protocol is shown below.

Consolidation protocol of the composite of pre-wetted glass fiber textiles and PLA powder.

Heat up press to 200 °C.

20 Place the mold in the press and use Teflon sheets to separate the mold from the press and apply 5 kN until the temperature within the mold is 195 °C.

Apply 20 kN during 5 minutes

Apply 30 kN during 5 minutes

Cool down the press to 20 °C, while the applied force is maintained at 30 kN

25 Take the mold out of the press and open it

Example III

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The steps that were carried out to make a composite of filament wound continuous glass fiber and PLA is listed below.

The fiber volume fraction, the mass of PLA, the shift between fibers, and the number of layers were defined, considering the trade-off between shift, fiber volume fraction, and thickness of the final composite. The goal was to produce two plates of 150x150x1.4 mm with a fiber volume fraction of 0.4. Therefore, a total of 23 layers was needed with a distance of 1.5 mm between the fibers and 2 times 33.9 g PLA.

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- 2. Three layers of glass fiber with a tex-value of 136 g/km were filament wound around a winding mold with a shift of 1.5 mm.
- 3. A solution of 11.0 g of PLA in 170 mL chloroform was prepared.
- 4. A layer of this solution was applied to one side of the wound structure and dried for one hour.
- 5. A layer of this solution was applied to the other side of the wound structure and dried for one hour.
- 6. The two obtained plates were cut out.

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- 7. The rest of the solution was applied to both sheets on both sides with a brush.
- 10 8. The following layers were produced according to the procedure described above under numbers 2-7. These fiber layers were treated with a solution of 14.2 g PLA dissolved in approximately 200 mL chloroform, which was applied to the fibers.
 - 9. The obtained layers were placed in the mold in two stacks. The direction of one layer was different from the previous or next layer to obtain a 0°-90°-0°-:::- 0 ° ply sequence.
 - 10. The mold was closed and the composite was consolidated according to the protocol shown below.
- 20 <u>Consolidation protocol of the composite of filament wound glass fibers and PLA.</u> Heat up press to 200 °C.

Place the mold in the press and use Teflon sheets to separate the mold from the press Close the press and apply 5 kN until the temperature in the mold is 195 °C.

Apply 20 kN during 5 minutes

25 Apply 30 kN during 5 minutes

Cool down the press to 20 °C, while the applied force is maintained at 30 kN

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<u>Table A</u>
Overview of the flexural properties and the quality of all prepared and tested composites.

Example/	Volume	Flexural	Flexural	Failure mode	Adhesion
Experiment	Fraction	Modulus of	Strength of the		
	of fibers	Composite	Composite		
		(GPa)	(MPa)		
Α	0.62	29.6	334.4	Delamination	2
В	0.53	20.4	362.5	Delamination and	2
				fiber fracture	
I	0.59	33.0	453.1	Fiber fracture	2
II	0.44	18.5	408.9	Fiber fracture	2
III	0.42	26.4	487.7	Fiber fracture	2

The adhesion was categorized in four groups: 0 = no matrix in between fibers or on loose fibers; 1 = matrix present in between fibers, but not on loose fibers; 2 = matrix present in between fibers, and some matrix sticking to loose fibers; 3 = matrix present in between fibers and a lot of matrix is sticking to loose fibers.

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The goal of the examples was to prepare a biodegradable composite with a flexural stiffness, as shown by the flexural modulus, and flexural strength comparable to that of bone. The flexural stiffness of bone is 20-40 GPa; the flexural strength of bone is about 200 MPa.

The flexural strength of the composite should preferably be higher than the flexural strength of bone to limit the risk of failure of the implant.

It is clear from the examples that a biodegradable composite, wherein the glass fiber was pre-treated with a solution of PLA, has a much higher flexural strength when compared to a composite prepared from a glass fiber which is not pre-treated.

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CLAIMS

- Biodegradable composite comprising a biodegradable polymer and 20-70 vol% glass fibers, wherein the biodegradable composite has a flexural strength between 100 and 600 MPa.
- 2. Biodegradable composite according to claim 1, wherein the biodegradable composite has a flexural modulus between 10 and 40 GPa.
- 3. Biodegradable composite according to claim 1 or 2, wherein the glass fibers are continuous glass fibers.
- 10 4. Biodegradable composite according to any one of claims 1-3, wherein the glass fibers have a SiO₂ content of 15-60 wt%.
 - 5. Biodegradable composite according to any one of claims 1-4, wherein the glass fibers are resorbable glass fibers.
- Biodegradable composite according to any one of claims 1-5, wherein the
 biodegradable polymer comprises a poly(α-ester) or copolymers thereof.
 - 7. Biodegradable composite according to any one of claims 1-6, wherein the biodegradable polymer is poly(lactic acid).
 - 8. Process for the preparation of a biodegradable composite according to anyone of claims 1-7, wherein
 - a. the glass fibers are pre-treated with a solution of the biodegradable polymer in a solvent;
 - b. the solvent is evaporated;
 - c. the pre-treated glass fibers, optionally together with additional biodegradable polymer, is placed in a mold, where after the biodegradable polymer present on the fibers and/or added to the mold is melted by applying heat and pressure;
 - d. the mold is cooled and the biodegradable composite is removed from the mold.
- 9. Process according to claim 8, wherein the biodegradable polymer used for the pretreatment of the glass fibers is the same as the biodegradable polymer added to the mold.
 - 10. Medical implant comprising a biodegradable composite according to claim 1-6, wherein the medical implant is chosen from a screw, a pin, a plate, a suture, a mesh, a net, a film, a tube, a balloon, a bag, a rod, an anchor, a valve, a ring,

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a stent, a cage, a spacer, a graft, a porous or open structure, a scaffold and/or components thereof.

International application No

PCT/EP2010/056026 A. CLASSIFICATION OF SUBJECT MATTER INV. B29C70/02 A61F2 A61F2/30 A61L27/44 A61L27/58 ADD. According to International Patent Classification (IPC) or to both national classification and IPC **B. FIELDS SEARCHED** Minimum documentation searched (classification system followed by classification symbols) B29C A61F A61L Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched Electronic data base consulted during the international search (name of data base and, where practical, search terms used) EPO-Internal, WPI Data C. DOCUMENTS CONSIDERED TO BE RELEVANT Category* Citation of document, with indication, where appropriate, of the relevant passages Relevant to claim No. X US 6 344 496 B1 (NIEDERAUER GABRIELE [US] 1-7,10ET AL) 5 February 2002 (2002-02-05) column 1, line 11 - line 54 column 3, line 10 - line 18 column 4, line 1 - line 26 claims 1-10 X EP 1 872 806 A1 (VIVOXID OY [FI]) 1-7,102 January 2008 (2008-01-02) paragraph [0001] paragraph [0004] paragraph [0021] - paragraph [0022] paragraph [0024] paragraph [0042] - paragraph [0044] paragraph [0046] - paragraph [0053] Further documents are listed in the continuation of Box C. See patent family annex. Special categories of cited documents: "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the "A" document defining the general state of the art which is not considered to be of particular relevance invention earlier document but published on or after the international "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another "Y" document of particular relevance; the claimed invention citation or other special reason (as specified) cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled document referring to an oral disclosure, use, exhibition or other means document published prior to the international filing date but in the art. later than the priority date claimed "&" document member of the same patent family Date of the actual completion of the international search Date of mailing of the international search report 4 August 2010 16/08/2010 Name and mailing address of the ISA/ Authorized officer European Patent Office, P.B. 5818 Patentlaan 2

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C(Continua	tion). DOCUMENTS CONSIDERED TO BE RELEVANT	PC1/EP2010/056026
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2005/226904 A1 (CH0I H00N [US] ET AL) 13 October 2005 (2005-10-13) paragraph [0003] paragraph [0020] - paragraph [0022] paragraph [0025] - paragraph [0026] paragraph [0058] - paragraph [0061] figure 1	1-3
X	WO 2008/112912 A (SMITH & NEPHEW INC [US]; AUSTIN GENE EDWARD [US]; BETTENGA MASON [US];) 18 September 2008 (2008-09-18) paragraph [0009] - paragraph [0011] paragraph [0144] paragraph [0181] paragraph [0216] - paragraph [0217] paragraph [0221] - paragraph [0223]	8,9
A	WO 90/00410 A (BIOCON OY [FI]) 25 January 1990 (1990-01-25) page 1, line 4 - line 13 page 4, line 36 - page 5, line 20 page 10, line 18 - line 38 page 12, line 13 - line 28 page 16, line 6 - line 23	1,6-10
A	US 6 031 148 A (HAYES BYRON KENT [US] ET AL) 29 February 2000 (2000-02-29) column 1, line 10 - line 12 column 4, line 64 - column 5, line 35 column 7, line 4 - line 46	1,6-8
A	US 5 522 895 A (MIKOS ANTONIOS G [US]) 4 June 1996 (1996-06-04) column 1, line 5 - line 12 column 1, line 28 - line 33 column 2, line 47 - line 67 column 3, line 30 - line 47 column 4, line 1 - line 12 column 4, line 59 - column 5, line 35	1-10
A	US 6 197 410 B1 (VALLITTU PEKKA [FI] ET AL) 6 March 2001 (2001-03-06) column 1, line 8 - line 48 column 4, line 66 - column 6, line 36	1-10

Information on patent family members

International application No
PCT/EP2010/056026

	ent document n search report		Publication date		Patent family member(s)		Publication date
US 6	5344496	B1	05-02-2002	AU CA EP JP JP WO US	6970298 2286074 1018978 2002508677 2007301382 9846164 5977204	A1 A1 T A A1	11-11-1998 22-10-1998 19-07-2000 19-03-2002 22-11-2007 22-10-1998 02-11-1999
EP 1	872806	A1	02-01-2008	NONE			
US 2	2005226904	A1	13-10-2005	NONE			
WO 2	2008112912	A	18-09-2008	EP	2131879	A2	16-12-2009
WO 9	0000410	Α	25-01-1990	AT AU CA DE DE EP FI JP	113484 615577 4236789 1341080 68919221 68919221 0423155 883197 2909116 3505535	B2 A C D1 T2 A1 A B2	15-11-1994 03-10-1991 11-04-1991 08-08-2000 08-12-1994 08-06-1995 24-04-1991 06-01-1990 23-06-1999 05-12-1991
US 6	031148	A	29-02-2000	CA DE DE EP JP WO	2094908 69121587 69121587 0560934 6506366 9210218	D1 T2 A1 T	07-06-1992 26-09-1996 27-03-1997 22-09-1993 21-07-1994 25-06-1992
US 5	522895	Α	04-06-1996	AU WO	7402894 9503011		20-02-1995 02-02-1995
US 6	197410	B1	06-03-2001	AT AU BR CA CN CZ DE DE DK EE	288251 754714 2427599 9908689 2322891 1299264 20003166 69923549 69923549 1067895 200000523	B2 A A A1 A A3 D1 T2 T3	15-02-2005 21-11-2002 27-09-1999 14-11-2000 16-09-1999 13-06-2001 17-01-2001 10-03-2005 16-02-2006 23-05-2005 15-02-2002
US 6	197410	B1		EP ES FI WO HU JP NO NZ PL PT RU	1067895 2235460 980528 9945890 0102583 2002506086 20004475 507401 342769 1067895 2207107	T3 A A1 A2 T A A A1 E	17-01-2001 01-07-2005 10-09-1999 16-09-1999 28-11-2001 26-02-2002 08-11-2000 25-10-2002 02-07-2001 29-04-2005 27-06-2003

Information on patent family members

International application No
PCT/EP2010/056026

Patent document cited in search report	Publication date	Patent family member(s)		Publication . date
		SK	13302000 A3	12-02-2001
				!