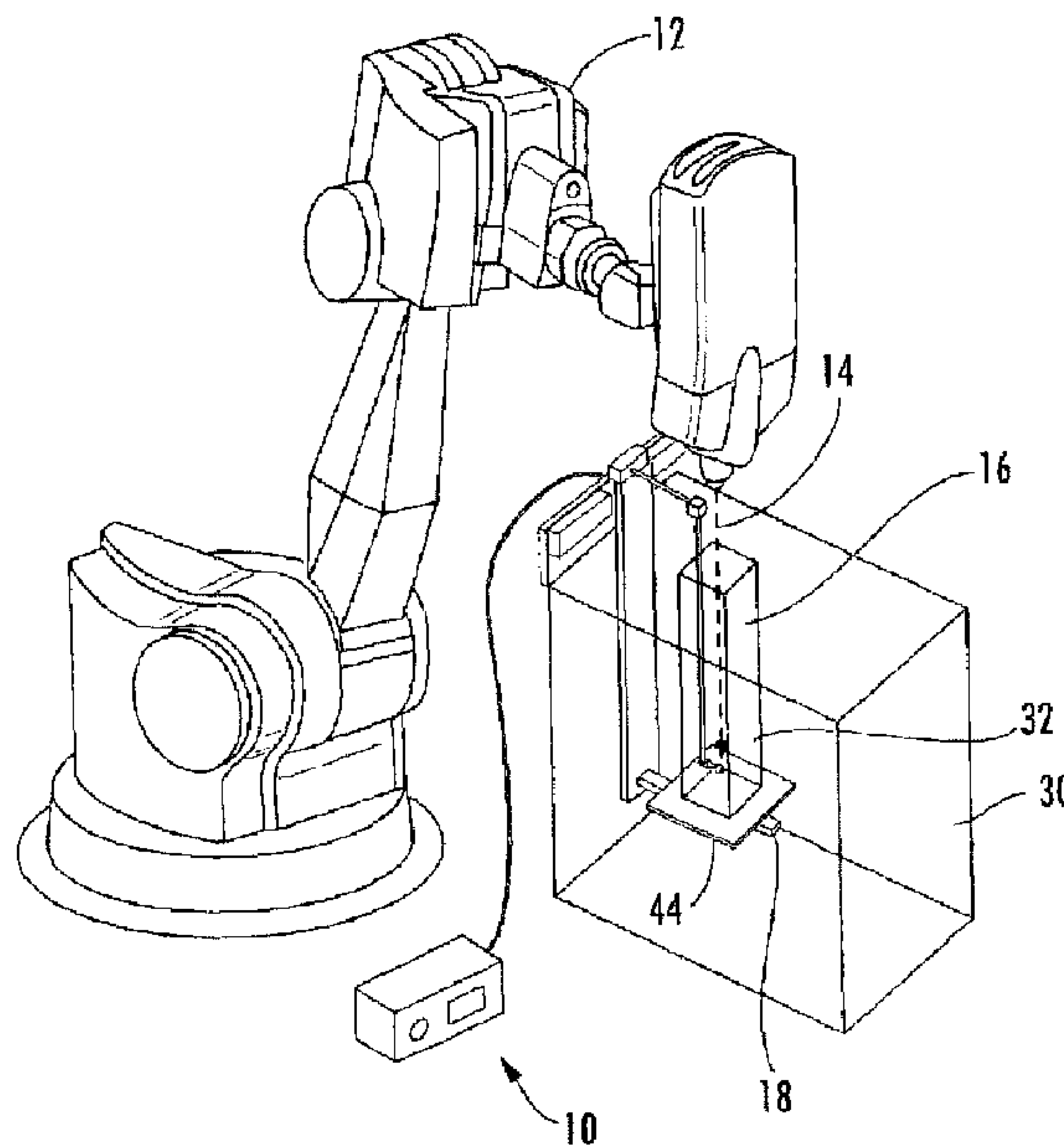




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(57) **Abrégé/Abstract:**

A radiation beam analyzer for measuring the distribution and intensity of radiation produced by a CyberKnife®. The analyzer employs a relative small tank of water into which a sensor is placed. The distance between the sensor and the radiation source is not varied. The tank of water is raised and lowered relative to the sensor to simulate the location of a malady within a patient's body. This movement of the tank permits the radiation from the CyberKnife® to be properly calibrated and adjusted for a proper treatment of a malady in a patient. In a second embodiment a radiation beam analyzer measures the distribution and intensity of radiation produced by a radiation source. The analyzer employs a relative small tank of water into which a sensor or detector is placed. The distance between the sensor and the radiation source is not varied. There are two methods to maintain the SAD (source to axis distance) constant. A first method maintains the position of detector fixed, utilizing a holder designed to retain the detector, and raises or lowers the small tank of water. A second method moves the detector up or down with a raising and lower mechanism in one direction and synchronically moves the small tank of water in the opposite direction with another raising and lowering mechanism. The second method also keeps the SAD constant. These methods position the detector relative to the radiation source to simulate the location of a malady within a patient's body. This movement of the tank permits the radiation from the radiation beam source to be properly isocentrically measured.

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## RADIATION BEAM ANALYZER AND METHOD

### FIELD OF THE INVENTION

This invention relates to a method and device for measuring the radiation dose of a linear accelerator or other radiation producing device at a target, and particularly relates to the tracking and measurement of a radiation dose from a Cyberknife®, a linear accelerator or other radiation producing devices used in conjunction with a radiosurgery system for the non-invasive treatment of both cancerous and non-cancerous tumors anywhere in the human body including the prostate, lung, brain, spine, liver pancreas and kidney.

### BACKGROUND OF THE INVENTION

Various well known medical techniques for the treatment of malignancies involve the use of radiation. Radiation sources, for example medical linear accelerators, are typically used to generate radiation which is directed to a specific target area of a patient. Proper doses of radiation directed at the malignant area of the patient are of the utmost importance. When properly applied, the radiation produces an ionizing effect on the malignant tissues of the patient, thereby destroying the malignant cells. As long as the dosimetry of the applied radiation is properly monitored, the malignancy can be treated without any detriment to the surrounding healthy body tissue. The goal of these treatments is to focus a high dose of radiation to a tumor or malignant cells while minimizing the exposure of the surrounding healthy tissue to the radiation. Accelerators may be utilized to deliver the radiation. Different accelerators have varying characteristics and output levels. The most common type of accelerator produces pulse radiation. The output beam has a rectangular shape in cross section and a cross sectional area typically between 1 and 1,600 square centimeters (cm<sup>2</sup>). Preferably the cross sectional area or field size is between 1 x 1 square centimeters (cm<sup>2</sup>) and 40 x 40 square centimeters (cm<sup>2</sup>). Rectangular or square cross sectional shapes are often changed to any desired cross sectional shape using molded or cast lead or cerrobend materials. More advanced accelerators use multi-leaf collimators. Other accelerators are continuously or non-pulsed such as cobalt radiation machines. Some accelerators utilize a swept electron beam, which passes a very narrow electron beam across the treatment field by means of varying electromagnetic fields.

To ensure proper dosimetry, linear accelerators used for the treatment of malignancies must be calibrated. Both the electron and photon radiation must be appropriately measured and correlated to the particular device. The skilled practitioner must insure that both the intensity and duration of the radiation treatment is carefully calculated and administered so as to produce the therapeutic result desired while maintaining the safety of the patient. Parameters such as flatness, symmetry, radiation and light field alignment are typically determined. The use of too much radiation may, in fact, cause side effects and allow destructive effects to occur to the surrounding tissue. Use of an insufficient amount of radiation will not deliver a dose that is effective to eradicate the malignancy. Thus, it is important to be able to determine the exact amount of radiation that will be produced by a particular machine and the manner in which that radiation will be distributed within the patient's body.

In order to produce an accurate assessment of the radiation received by the patient, at the target area, some type of pattern or map of the radiation at varying positions within the patient's body must be produced. These profiles correlate: 1) the variation of dose with depth in water generating percent depth dose profiles, 2) the variation of dose across a plane perpendicular to the radiation source generating the cross beam profiles, and 3) the variation of dose with depth in water generating percent depth dose and TMR/TPR (Tissue Maximum Ratio/Tissue Phantom Ratio) when the SAD (source to axis distance) is constant profiles. These particular measurements of cross beam profiles are of particular concern in the present invention. Although useful for other analyses, the alignment of the cross profiles in both radial and transverse planes is the basis of the present invention.

There are companies that provide the calibration service to hospitals and treatment centers. These physicists must visit the facility and conduct the calibration of the radiation source with their own equipment. This requires lightweight, easily portable, less cumbersome radiation measuring devices that can be quickly assembled and disassembled on site. The actual scanning should also be expeditious with the results available within a short time frame. Such equipment allows a physicist to be more efficient and calibrate more radiation devices in a shorter period of time.

One existing system for measuring the radiation that is produced by medical linear accelerators utilizes a large tank on the order of 50cm x 50cm x 50cm filled with water. A group of computer controlled motors move the radiation detector through a series of pre-programmed steps along a single axis beneath the water's surface. Since the density of the human body closely approximates that of water, the water-filled tank provides an appropriate medium for creating a simulation of both the distribution and the intensity of radiation which would likely occur within the patient's body. The aforementioned tank is commonly referred to as a water phantom. The radiation produced by the linear accelerator will be directed into the water in the phantom tank, at which point the intensity of the radiation at varying depths and positions within the water can be measured with the radiation detector. As the radiation penetrates the water, the direct or primary beam is scattered by the water, in much the same way as a radiation beam impinging upon the human patient. Both the scattered radiation, as well as the primary radiation are detected by the ion-chamber, which is part of the radiation detector or by radiation sensitive diodes.

The ion-chamber is essentially an open air capacitor which produces an electrical current that corresponds to the number of ions produced within its volume. The detector is lowered to a measurement point within the phantom tank and measurements are taken over a particular time period. The detector can then be moved to another measurement point where measurements are taken as the detector is held in the second position. At each measuring point a statistically significant number of samples are taken while the detector is held stationary.

In radiation therapy and radiosurgery, for example, a tumor may be non-invasively destroyed by a beam of ionizing radiation that kills the cells in the tumor. It is desirable to direct the radiation beam only to the tumor and not to the healthy tissue which surrounds the tumor. Therefore, accurate aiming of the beam at the tumor is extremely important in these radiation treatments. The goal is to focus a high dose of radiation to the tumor while minimizing the exposure of the surrounding healthy tissue to radiation. For adequate distribution of radiation dosage to the tumor, the direction of the radiation beam is typically adjusted during the treatment to track the tumor.

The most advanced modern radiosurgery systems, such as the Cyberknife® Robotic Radiosurgery System of Accuray, Inc., utilizes stereo online x-ray imaging during treatment to enhance the accuracy of the radiation treatment. The position of a patient's bony landmarks, e.g. their skull, can be determined with high accuracy by using the Cyberknife® stereo x-ray camera system. Thus, this highly accurate x-ray camera system can be used to treat a target region if the position of the target region relative to a bony landmark remains constant. However, the x-ray camera system cannot be used to determine the position of a target region if the position of the target region relative to a bony landmark changes because the target, e.g. a tumor, is generally not visible in x-ray images. For example, a target region in a patient's abdomen or chest cannot be treated with this method alone.

An image guidance system is essential to the proper operation of the Cyber Knife® system. The first method developed for controlling the image guidance system was known as 6D or skull based tracking. An X-ray camera produces images which are compared to a library of computer generated images of the patient anatomy Digitally Reconstructed Radiographs (DRR's) and a computer algorithm determines what motion corrections have to be given to the robot because of patient movement. This imaging system allows the CyberKnife® to deliver radiation with an accuracy of 0.5mm without using mechanical clamps attached to the patient's skull. The use of the image guided technique is referred to as frameless stereotactic radiosurgery. This method is referred to as 6D because corrections are made for the 3 translational motions (X, Y and Z) and three rotational motions.

#### DESCRIPTION OF THE PRIOR ART

Several prior art devices are known to teach systems for ascertaining the suitable dosimetry of a particular accelerator along with methods for their use.

U.S. Pat. Nos. 5,621,214 and 5,627,367, to Sofield, are directed to a radiation beam scanner system which employs a peak detection methodology. The device includes a single axis mounted within a water phantom. In use, the water phantom must be leveled and a reference detector remains stationary at some point within the beam while the signal detector is moved up and down along the single axis by the use of electrical stepper motors. While these devices employ a water phantom, they are limited to moving the signal detector along the single axis and can only provide a planar scan of the beam.

U.S. Patent Application Publication 2006/0033044 A1, to Gentry et al., is directed to a treatment planning tool for multi-energy electron beam radiotherapy. The system consists of a stand-alone calculator that enables multi-energy electron beam treatments with standard single electron beam radio-therapy equipment thereby providing improved dose profiles. By  
5 employing user defined depth-dose profiles, the calculator may work with a wide variety of existing standard electron beam radiotherapy systems.

U.S. Pat. No. 6,225,622, issued May 1, 2001, to Navarro, the inventor here, describes a dynamic radiation measuring device that moves the ion chamber through a stationary radiation beam to gather readings of radiation intensity at various points within the area of  
10 the beam. The disclosure of this patent may be referred to for further details.

U.S. Pat. No. 4,988,866, issued January 29, 1991, to Westerlund, is directed toward a measuring device for checking radiation fields from treatment machines used for radiotherapy. This device comprises a measuring block that contains radiation detectors arranged beneath a cover plate, and is provided with field marking lines and an energy filter.  
15 The detectors are connected to a read-out unit for signal processing and presentation of measurement values. The dose monitoring calibration detectors are fixed in a particular geometric pattern to determine homogeneity of the radiation field. In use, the measuring device is able to simultaneously check the totality of radiation emitted by a single source of radiation at stationary positions within the measuring block.

U.S. Patent Application Publication 2005/0173648 A1, to Schmidt et al., is directed to a wire free, dual mode calibration instrument for high energy therapeutic radiation. The apparatus includes a housing with opposed first and second faces holding a set of detectors between the first and second faces. A first calibrating material for electrons is positioned to intercept electrons passing through the first face to the detectors, and a second calibrating  
25 material for photons is positioned to intercept photons passing through the second face to those detectors.

These devices do not use a water phantom and are additionally limited in that all of the ionization detectors are in one plane. This does not yield an appropriate three-dimensional assessment of the combination of scattering and direct radiation which would  
30 normally impinge the human body undergoing radiation treatment. Thus, accurate dosimetry in a real-life scenario could not be readily ascertained by the use of these devices.

U.S. Pat. No. 5,006,714, issued April 9, 1991, to Attix, utilizes a particular type of scintillator dosimetry probe which does not measure radiation directly but instead measures the proportional light output of a radiation source. The probe is set into a polymer material that approximates water or muscle tissue in atomic number and electron density. Attix  
5 indicates that the use of such a detector minimizes perturbations in a phantom water tank.

Additionally, there is an apparatus called a Wellhofer bottle-ship which utilizes a smaller volume of water than the conventional water phantom. The Wellhofer device utilizes a timing belt and motor combination to move the detector through the water, thus requiring a long initial set-up time.

10 Thus, there exists a need for a portable, modular radiation beam measuring device. The device should be capable of rapid assembly and disassembly for use at various locations to calibrate various CyberKnife® systems. The device should be capable of repeatable, accurate detection of the radiation emitted from the CyberKnife®. Since the distance between the CyberKnife and the item being treated, e.g. a tumor, remains constant with this  
15 system, the device should also utilize a relative small volume of water or other fluid.

None of the above prior art devices are capable of performing fast and accurate isocentric measurements that result in direct measurement of the TMR/TPR (Tissue Maximum Ratio/ Tissue Phantom Ratio) in depth and isocentric cross profiles. There also exists a need for a portable, modular radiation beam measuring device. The device should be  
20 capable of rapid assembly and disassembly for use at various locations to calibrate various isocentric radiation beam systems. The device should be capable of repeatable, accurate detection of the radiation emitted from the radiation source. Since the distance between the isocentric radiation beam source and the item being treated, e.g. a tumor, remains constant with this system, the device should also be capable of utilizing a relative small volume of  
25 water.

#### SUMMARY OF THE INVENTION

A first embodiment of the invention embodies a radiation beam analyzer for measuring the distribution and intensity of radiation produced by the CyberKnife®. The analyzer employs a relative small tank of water into which a sensor is placed. The distance  
30 between the sensor and the radiation source is not varied. The tank of water is raised and lowered relative to the sensor to simulate the location of a malady within a patient's body.

This movement of the tank permits the radiation from or the CyberKnife® to be properly calibrated and adjusted for a proper treatment of a malady in a patient.

Another embodiment of the invention embodies a radiation beam analyzer for measuring the distribution and intensity of radiation produced by a radiation source. The analyzer employs a relative small tank of water into which a sensor or detector is placed.

The distance between the sensor and the radiation source is not varied. There are two methods to maintain the SAD (source to axis distance) constant. A first method maintains the position of detector fixed, utilizing a holder designed to retain the detector, and raises or lowers the small tank of water. A second method moves the detector up or down with a raising and lowering mechanism in one direction and synchronically moves the small tank of water in the opposite direction with another raising and lowering mechanism. The second method also keeps the SAD constant. These methods position the detector relative to the radiation source to simulate the location of a malady within a patient's body. This movement of the tank permits the radiation from the isocentric radiation beam source to be properly isocentrically measured.

In yet another embodiment, the invention contemplates a radiation beam analyzer for detecting radiation dosimetry of a beam emitted along an axis from a radiotherapy treatment device that includes a dynamic phantom body formed of a material having a density proximal that of a human body, a tank containing the dynamic phantom body, at least one dosimetry probe constructed and arranged to sense photons and electrons positioned within the dynamic phantom body, a carriage supporting the tank and the dynamic phantom body, a guideway to which the carriage is secured, a first mechanism incrementally moving the carriage, the tank and the dynamic phantom body relative to the guideway in a X-axis, a Y-axis and a Z-axis, where the X-axis, Y-axis and Z-axis are orthogonal to each other, a second mechanism incrementally moving the at least one dosimetry probe within the dynamic body relative to the tank, and a controller connected to and operating the first and the second mechanisms simultaneously to move both the tank and the dosimetry probe relative to each other to maintain the distance between a radiation source and the axis of a beam emitted from the radiation source to the dosimetry probe constant. Movement of the dynamic phantom body through a series of locations is carried out so as to provide sufficient data to determine the proper dose of radiation required for radiotherapy treatment.

In still another embodiment, the invention contemplates a method of calibrating a radiotherapy treatment device that includes the steps of providing a source of radiation along an axis, providing a dynamic phantom body formed of a material having a density proximally that of a human body, providing a tank containing the dynamic phantom body, providing at least one dosimetry probe constructed and arranged to sense photons and electrons, positioning the dosimetry probe within the dynamic phantom body, supporting the dynamic phantom body and the tank on a carriage, securing the carriage to a guideway, incrementally moving the carriage, the tank and the dynamic phantom body relative to the guideway in a X-axis, a Y-axis and a Z-axis where the X-axis, the Y-axis and the Z-axis are orthogonal to each other, incrementally moving the dosimetry probe within the dynamic body relative to the tank, and employing a controller to simultaneously move both the tank and the dosimetry probe relative to each other to maintain the distance between a radiation source and the axis of a beam emitted from the radiation source to the dosimetry probe constant. Movement of the dynamic phantom body through a series of locations is carried out so as to provide sufficient data to determine the proper dose of radiation required for radiotherapy treatment.

Accordingly, an aspect of the instant invention seeks to provide an accurate measurement of the radiation from a linear accelerator or the CyberKnife® used to perform radiosurgery or to treat a malady.

A further aspect of the instant invention seeks to accurately position a linear accelerator or the CyberKnife® relatively to a malady in a patient's body.

Yet another aspect of the instant invention seeks to provide a modular radiation device including a relatively small tank of water which is moved relative to a fixed sensor in order to determine the proper amount of radiation required to treat a malady.

Still a further aspect of the invention seeks to provide a system and method for electronically controlling the movement of a tank of water and the measurement of radiation from a CyberKnife®.

A further aspect of the instant invention seeks to accurately position the radiation detector as well as obtain high repeatability of the measurements.

Yet another aspect of the instant invention seeks to provide a modular radiation device including a relatively small tank of water which is moved relative to a fixed detector or sensor in order to determine the proper amount of radiation required to treat a malady.

Still a further aspect of the invention seeks to provide a system and method for electronically controlling the movement of a relatively small tank of water and the movement of a detector or sensor mounted within the tank for the measurement of radiation from an isocentric radiation beam source.

5 Other aspects and advantages of this invention will become apparent from the following description taken in conjunction with any accompanying drawings wherein are set forth, by way of illustration and example, certain embodiments of this invention. Any drawings contained herein constitute a part of this specification and include exemplary embodiments of the present invention and illustrate various aspects and features thereof.

10 BRIEF DESCRIPTION OF THE FIGURES

FIGURE 1 is a perspective view of the present invention in use measuring the radiation from a CyberKnife®;

FIGURE 2 is a front view of the present invention;

FIGURE 3 is a side view of the present invention;

15 FIGURE 4 is a top perspective view of the present invention;

FIGURE 5 is an enlarged front view of the present invention;

FIGURE 6 is an enlarged front perspective view of only the measurement tank of the present invention;

20 FIGURE 7 is a perspective view of the prior art radiation treatment system utilizing an isocentric radiation beam source to treat a patient;

FIGURE 8 is a front view of a second embodiment of the present invention incorporating the small tank and with the detector in a raised position;

FIGURE 9 is a front view of a second embodiment of the present invention incorporating the small tank and with the sensor in a lowered position;

25 FIGURE 10 is a side view of a second embodiment of the present invention incorporating the small tank with the detector in a raised position;

FIGURE 11 is a side view of the small tank of a second embodiment of the present invention with the detector in a raised position;

30 FIGURE 12 is a side view of the small tank of a second embodiment of the present invention with the detector in a lowered position;

FIGURE 13 is a rear perspective view of the small tank of a second embodiment of the present invention with the detector in a raised position;

FIGURE 14 is a rear perspective view of the small tank of a second embodiment of the present invention with the detector in a lowered position;

5 FIGURE 15 is a perspective view of a second embodiment of the present invention in use measuring the radiation from an isocentric radiation beam source;

FIGURES 16A and 16B are the results of an isocentric depth scan (TMP) and a cross profile;

FIGURE 17 is a perspective view of a third embodiment of the present invention;

10 FIGURE 18 is an end view of a third embodiment of the present invention;

FIGURE 19 is a front view of a third embodiment of the present invention and

FIGURE 20 is a top view of a third embodiment of the present invention.

#### DETAILED DESCRIPTION OF THE INVENTION

15 While the present invention is susceptible of embodiment in various forms, there is shown in the drawings and will hereinafter be described a presently preferred, albeit not limiting, embodiment with the understanding that the present disclosure is to be considered an exemplification of the present invention and is not intended to limit the invention to the specific embodiments illustrated.

20 The present invention is designed to measure with accuracy, precision and speed the radiation beams produced by a CyberKnife®. The Dynamic Phantom and Direct TMP/TPR Direct Measurement of radiation from a device utilized in radiosurgery have been previously described in applicant's related patent publications referred to herein. A combination of these two measurement methods and modifications of some of the features of these measurement methods has resulted in the present invention which will be described  
25 hereinafter.

Although the two basic concepts of Dynamic Phantom and Direct TMR/TPR Direct measurements are the same, the present invention requires water, not solid water like the Dynamic Phantom and different from TMR/TPR. The radiation is imparted with the radiation source on the top of a tank, not laterally like in applicant's previous TMR/TPR  
30 measurements. The present invention also permits the use of a tank with a significantly

smaller capacity. In a preferred embodiment the tank's capacity is 2.5 liters versus a prior art tank's capacity of 100 liters.

Referring to Figs. 1-6, a first embodiment of the invention including a modular radiation beam analyzer 10 for measuring the distribution and intensity of radiation produced by a CyberKnife® 12 in a radiosurgery system is illustrated. A radiation beam 14 is emitted by a CyberKnife® in a substantially vertical direction. The beam 14 is very sharp and can be positioned on a patient with accuracy of less than one millimeter. The beam 14 is used to treat areas on a patient which preferably have a minimum field size of 0.5cm in diameter and a maximum field size of 6cm in diameter. The radiosurgery system, in which the CyberKnife® is employed, requires that all the radiation measurements be taken utilizing the isocentric method or direct measurement of TMR/ TPR (Tissue Maximum Ratio/ Tissue Phantom Ratio). In addition, because of the accuracy of this radiosurgery procedure, the measurements of the radiation require extreme accuracy.

The relatively small tank of the present invention is placed onto a carriage 18 of a measurement device which employs a substantially larger tank 30. The larger measurement device allows the carriage 18 to be moved in three different axes, X, Y and Z. The X axis extends along a horizontal portion of the tank 30 and can be seen in Fig. 2. The Y axis extends in the vertical direction and can also be seen in Fig. 2. The Z axis extends toward and away from a rear wall of the tank 30 and can be seen in Fig. 3. Small motors, such as a stepper motor, move the carriage 18 along all three axes. The present invention includes a second tank 16 that is movable in the Y direction only. While a stepper motor is a preferred embodiment, any type of motor or device which can move the carriage 18 along each of the three axes can be utilized.

In radiosurgery systems which utilize the CyberKnife®, the distance between the CyberKnife® and the malady being treated on a patient, such as a tumor, remains constant. Thus, in order to simulate the different positions or depths in a patient's body that the tumor or other malady being treated may be located, only the relative depth of the water, which simulates the depth of the item within a patient's body, needs to be varied. Once the correct depth or position within a patient's body is simulated by moving a sensor 32 to a specific depth in the water within the second tank 16 the amount of radiation from the CyberKnife®

can be regulated to properly treat the tumor or malady. The present invention accomplishes this by moving the second tank 16 vertically up and down along the Y axis.

The sensor 32 is mounted on or positioned within a support 34, Figs. 4, 5 and 6. The support 34 is secured onto a substantially vertical rod or support 36. The support 36 is in turn connected to and supported on a substantially horizontal rod or support 38. While a preferred connection device 40 is illustrated which applies a transverse force on supports 36 and 38, any other type of connection device 40 could also be employed. Support or rod 38 is connected to a guideway 42, Fig. 3, utilizing a connection device 44 mounted on the guideway. The support 34 permits the distance between the CyberKnife® 12 and the sensor 32 to be adjusted to simulate the distance between a commercial CyberKnife® and the malady being treated. The supports 38 and 34 permit the sensor 32 to be aligned with the radiation beam 14 from the CyberKnife® 12.

A stepper motor or other similar device (not shown) moves the carriage 18 along the Y axis. This simulates the depth or level into which a malady is located within a patient's body. The carriage 18 has a support plate or platform 44 secured thereon, Fig. 5. The lower portion of second tank 16 is removably secured to the platform 44 so that the tank will not fall off the carriage 18 during operation of the present invention. There are various methods of securing second tank 16 to platform 44 including but not limited to fastening, gluing, welding, etc. While in the preferred embodiment, the second tank 16 is releasably secured to platform 44; it could also be permanently attached thereto.

While the second tank 16 is illustrated as substantially square in cross section and rectangular in height, a preferred embodiment is cylindrical. The cylinder is preferably 19cm in diameter and 40cm high. It is made from a clear acrylic material. Tanks having various other dimensions and weights can also be utilized. Tanks can also be made from various other materials.

This embodiment of the present invention utilizes the software and programming disclosed in applicant's other U.S. patent application publications, in for example U.S. Patent Application Publication 2008/0048125 A1 published February 28, 2008, entitled, "Convertible Radiation Beam Analyzer System" to control the motors which operate the guideways, to acquire data, to analyze the data, to provide graphical representations of the data and to transfer data with the pertinent modifications.

This embodiment of the present invention can be used with a single or an array of ion chambers. It can also be used with a plurality of diodes. The present invention can also be utilized with conventional radiation therapy. When used with conventional radiation therapy the dimensions of the second tank 16 are 14cm long by 14cm wide by 40cm high.

5 Another embodiment of the present invention is designed to isocentrically measure with accuracy, precision and speed the radiation beams produced by a radiation beam source. This second embodiment of the present invention can also be used with a Cyberknife® radiation system. The dynamic phantom measurement of radiation and direct measurement of TMR/TPR (Tissue Maximum Ratio/ Tissue Phantom Ratio) functions from a device  
10 utilized in radiosurgery have been previously described in applicant's related patent publications referred to herein. A combination of these two measurement methods and modifications of some of the features of these measurement methods has resulted in the present invention which will be described hereinafter. An isocentric radiation treatment system maintains the distance between the radiation source and the malady of a patient  
15 constant. In other words the SAD (source to axis distance) is constant. The radiation source can also be pivoted around the patient utilizing a manipulator 116 as illustrated in Figs. 7 and 15.

There are two methods to maintain the SAD (source to axis distance) constant. A first method maintains the position of detector fixed, utilizing a holder designed to retain the  
20 detector, and raises or lowers the small tank of water. A second method moves the detector up or down with a raising and lowering mechanism in one direction and synchronically moves the small second tank of water in the opposite direction with another raising and lowering mechanism. The second method also keeps the SAD constant. These methods position the detector relative to the radiation source to simulate the location of a malady  
25 within a patient's body. This movement of the tank permits the radiation from the radiation beam source to be properly isocentrically measured.

Although the two basic concepts of dynamic phantom measurement and direct measurement of TMR/TPR functions are the same, this embodiment of the present invention can use water instead of solid water like the dynamic phantom measurement to measure  
30 cross beam profiles. This second embodiment of the present invention can also perform direct measurements of TMR/TPR with the radiation being imparted from source on the top

of a tank, not laterally like in applicant's previous TMR/TPR measurements. Finally, combining these two concepts it is possible with a single device to isocentrically measure relative depth dose (TMR/TPR) and cross beam profiles. With the previous inventions two different devices were required. This second embodiment of the present invention also  
5 permits the use of a tank of water with a significantly smaller capacity than employed in prior art measurement systems. In a preferred embodiment the tank's capacity is 2.5 liters versus a prior art tank's capacity of 100 liters.

Referring to Figs. 7-15, a prior art isocentric radiation treatment apparatus 110 is illustrated in Fig. 7. The isocentric radiation treatment apparatus illustrated in Fig. 7  
10 comprises a radiation generation unit 112, a variable collimator 114, a manipulator 116, a movable table 118, a diagnosis imager 120, and a control unit 122 which produces a radiation beam 124. The modular radiation beam analyzer 126 of the present invention for measuring the distribution and intensity of radiation produced by an isocentric radiation beam 124 in a radiosurgery system is illustrated in Fig. 15. The radiation beam 124 is emitted by an  
15 isocentric radiation beam source in a substantially vertical direction. The radiation beam 124 is very sharp and can be positioned on a patient with accuracy of less than one millimeter. The beam 124 is used to treat areas on a patient which preferably have a minimum field size of 0.5cm in diameter and a maximum field size of 6cm in diameter. The radiosurgery system, in which the isocentric radiation beam is employed, requires that all the radiation  
20 measurements be taken utilizing the isocentric method of direct measurement of TMR/TPR (Tissue Maximum Ratio/ Tissue Phantom Ratio) of the present invention. In addition, because of the accuracy of this radiosurgery procedure, the measurements of the radiation delivered to the patient require extreme accuracy.

The relatively small tank 128 of this second embodiment of the present invention is  
25 placed onto a carriage 130 of a measurement device. A portable folding frame 131 holds the whole system. The modular radiation beam analyzer 126 enables the carriage 130 to be moved in three different axes, X, Y and Z. The X axis extends in a horizontal direction along a portion of the tank 132 and is illustrated in Figs. 8 and 15. The Z axis extends in a vertical direction and can also be seen in Figs. 8 and 15. The Y axis extends toward and away from a  
30 rear wall of tank 132 and can be seen in Figs. 4 and 9. Small motors, such as a stepper motor, move the carriage 130 along all three axes. While a stepper motor is a preferred

embodiment, any type of motor or device which can move the carriage 118 along each of the three axes can be utilized.

This second embodiment of the present invention includes a small tank 128 which is movable in the Y direction and a detector or sensor 134 which is movable in the Y direction also. A small motor, such as a stepper motor 136, rotates a screw 138 in both a clockwise and counter clockwise direction, as illustrated in Figs. 11 and 12. A mounting support 140 holds and retains the detector or sensor 134 in a fixed position. The mounting support 140 is secured to and supported on the screw 138 such that when the screw rotates in one direction the mounting support 140 will be raised, relative to the bottom of the tank 132, and when the screw is rotated in the opposite direction the screw will be lowered. While a preferred mounting support 140 is illustrated which applies a transverse force on detector or sensor 134, any other type of mounting support 140 could also be employed. The mounting support 140 permits the distance between the isocentric radiation beam source 112 and the detector or sensor 134 to be adjusted to simulate the distance between a commercial isocentric radiation beam and the malady of an individual or patient to be treated utilizing the radiosurgery system described above. The mounting support 140 also permits the detector or sensor 134 to be aligned with the radiation beam 112 from the isocentric radiation beam source 112.

In radiosurgery systems which utilize the isocentric radiation beam, the distance between the isocentric radiation beam source 112 and the malady being treated on a patient, such as a tumor, remains constant. Thus, in order to simulate the different positions or depths in a patient's body that the tumor or other malady being treated may be located, only the relative depth of the water, which simulates the depth of the item within a patient's body, needs to be varied. Once the correct depth or position within a patient's body is simulated by moving detector or sensor 134 to a specific depth in the water within the tank 128, the amount of radiation from the radiation source can be regulated to properly treat the tumor or malady. This second embodiment of the present invention accomplishes this by utilizing one of two methods. The first method maintains the position of detector 134 fixed, utilizing a holder 140 designed to retain the detector, and raises or lowers the small tank of water 128. The second method moves the detector or sensor 134 up or down with a raising and lowering mechanism in one direction and synchronically moves the small tank of water in the opposite direction with another raising and lowering mechanism. The second method also keeps the

SAD constant. These methods position the detector relative to the radiation source to simulate the location of a malady within a patient's body. This movement of the tank permits the radiation from the isocentric radiation beam source to be properly isocentrically measured. Main difference between the two methods: The second method uses an extra  
5 motor, extending the scanning capability to three (3) axes X, Y, Z, therefore scanning in depth, and radial transverse and diagonal directions. The first method can scan only in depth and transverse directions.

The first method raises and/or lowers the tank of water 128 by raising and/or lowering the carriage 130 with stepper motors or similar devices capable of raising and/or lowering the  
10 carriage. The second method raises and/or lowers the detector or sensor 134 by raising and/or lowering the mounting support 140 utilizing a screw mechanism 138 and stepper motor 136 or similar device which can raise and/or lower the support. Simultaneously the tank 128 is raised and/or lowered by raising and/or lowering the carriage 130 as described herein above. The motor(s) or device(s) which raise and/or lower the mounting support 140  
15 and the motor(s) or device(s) which raise and/or lower the carriage 130 are synchronized to maintain the detector or sensor 134 in a fixed position relative to the radiation source. In other words to keep the SAD constant.

As illustrated, tank 128 is 8cm long, 8cm wide and 40cm high. It has a capacity of 2.5 liters. It is made from a clear acrylic material. In a preferred embodiment, the tank 128  
20 is cylindrical having a diameter of 19cm and a height of 40cm. Tanks having various other dimensions and weights can also be utilized. Tanks can also be made from various other materials.

A wire or cable 142 extends from the detector or sensor to a recording device to measure and record the amount of radiation delivered to a specific point by the radiation  
25 source. Another wire or cable 144 extends from a control box 146, Fig. 9. The control box controls the movement of the carriage 130 in the X, Y and Z directions. Another wire or cable 148 extends from the motor 136 to a control device 150. This control device synchronizes the movement between the carriage 130 and the mounting support 140 to maintain the detector or sensor in a position fixed relative to the radiation source.

This embodiment of the present invention utilizes the software and programming disclosed in applicant's other U.S. patent application publications, in for example U.S. Patent Application Publication 2008/0048125 A1 published February 28, 2008, entitled, "Convertible Radiation Beam Analyzer System" to control the  
5 motors which operate the guideways, to acquire data, to analyze the data, to provide graphical representations of the data and to transfer data with the pertinent modifications.

This embodiment of the present invention can be used with a single or an array of ion chambers. It can also be used with a single or an array of diodes. This embodiment of the present invention can also be utilized with Cyberknife® or conventional radiation therapy.  
10 When used with conventional radiation therapy the dimensions of the tank 128 are 14cm long by 14cm wide by 40cm high. But the main applications are measurements of small fields, like the ones used in Cyberknife® machines and stereotactic procedures.

When scanning in the Z direction, the isocentric scanning generates the TMR/TPR function. This is accomplished using either one of the two methods described herein before.  
15 This is different from a conventional scanner which does not keep the SAD constant and generates a PDD (percentage depth dose) function. It should also be noted that TMR (Tissue Maximum Ratio) cannot scan across profiles isocentrically. It is further noted that dynamic phantom measurements cannot scan depths isocentrically. Results of an isocentric depth scan (TMR) and cross profiles and illustrated in Figs. 16A and 16B.

Referring to Figs. 17-20, a third embodiment of the present invention will now be described. This third embodiment is used in the same manner as the first two embodiments to perform direct measurements of TMR/TPR\_SAD (equivalent to isocentric measurements) with the radiation being imparted from a source (not shown) on the top of the tank 228. The radiation source could be the same as 12 and 112, illustrated in Figs. 1 and 7 respectively.  
20 Tank 228 would be placed on a movable table similar to 118 to measure the distribution and intensity of the radiation beam in the radiosurgery system, as illustrated in Fig 7.

Tank 228 is movable laterally in the X direction and also can be rotated about the Z axis by a rotary table 229. The rotary table 229 is operated by a motor, not shown. A plurality of vertical supports 231 are mounted on rails 233. The rails 233 hold and position  
30 the vertical supports 231 relative to each other. The rails 233 are mounted on the rotary table 229 and enable the entire device to be rotated about the Z axis. A second set of rails 235 are

mounted on vertical supports 231 substantially parallel to and spaced vertically from rails 233. The second set of rails 235 provides a support for tank 228.

An automated mechanism moves tank 228 in the X direction. This enables the detector or sensor 234 to be moved laterally along the X axis. Alternatively, a connection  
5 device 242 can be move along guideway 244. This can be accomplished automatically or manually. This also moves the detector 234 along the X axis. The detector or sensor 234 is mounted on a support 240. The support 240 can be moved vertically up and down along the Z axis either automatically or manually.

The third embodiment enables measurements of substantially larger fields than the  
10 first two embodiments without the use of a large tank of water. This is accomplished by rotating tank 228 up to 90 degrees from a first position to a second position. This movement enables detector 234 to be moved over a substantially larger area without employing a large tank. The use of the smaller tank 228 on a rotary base results in a significant reduction in the size of the tank and volume of water required to make measurements in large fields. This  
15 also results in a significant weight savings because of the relative small volume of water used: 11 gallons vs. 45 gallons in a conventional tank. A preferred tank is 35 cm long, 30 cm wide, 40 cm high and made from an acrylic material.

All patents and publications mentioned in this specification are indicative of the levels of those skilled in the art to which the invention pertains and may be referred to for  
20 further details.

It is to be understood that while a certain form of the invention is illustrated, it is not to be limited to the specific form or arrangement herein described and shown. It will be apparent to those skilled in the art that various changes may be made without departing from  
25 the scope of the invention and the invention is not to be considered limited to what is shown and described in the specification and any drawings/figures included herein.

One skilled in the art will readily appreciate that the present invention is well adapted to carry out the objectives and obtain the ends and advantages mentioned, as well as those inherent therein. The embodiments, methods, procedures and techniques described herein  
30 are presently representative of the preferred embodiments, are intended to be exemplary and are not intended as limitations on the scope. Changes therein and other uses will occur to

those skilled in the art which are encompassed within the scope of the invention as defined by the appended claims. Although the invention has been described in connection with specific preferred embodiments, it should be understood that the invention as claimed should not be unduly limited to such specific embodiments. Indeed, various  
5 modifications of the described modes for carrying out the invention which are obvious to those skilled in the art are intended to be within the scope of the following claims.

**What is claimed is:**

1. A radiation beam analyzer for detecting radiation dosimetry of a beam emitted along an axis from a radiotherapy treatment device comprising:

a dynamic phantom body formed of a material having a density proximal that of a human body;

a tank containing said dynamic phantom body;

at least one dosimetry probe constructed and arranged to sense photons and electrons, said at least one dosimetry probe positioned within said dynamic phantom body;

a carriage supporting said tank and said dynamic phantom body;

a guideway, said carriage secured to said guideway;

a first mechanism incrementally moving said carriage, said tank and said dynamic phantom body relative to said guideway in a X-axis, a Y-axis and a Z-axis, said X-axis, Y-axis and Z-axis are substantially orthogonal to each other;

a second mechanism incrementally moving said at least one dosimetry probe within said dynamic body relative to said tank; and

a controller connected to and operating said first and said second mechanisms simultaneously to move both said tank and said at least one dosimetry probe relative to each other to maintain the distance between a radiation source and the axis of a beam emitted from the radiation source to said at least one dosimetry probe constant;

whereby movement of said dynamic phantom body through a series of locations is carried out so as to provide sufficient data to determine the proper dose of radiation required for radiotherapy treatment.

2. The radiation scanning system of claim 1 wherein said dosimetry probe is an ion chamber.

3. The radiation scanning system of claim 1 wherein said dynamic phantom body includes a tank made from an acrylic material.

4. The radiation scanning system of claim 1 wherein said movement is isocentric.

5. The radiation scanning system of claim 1 wherein said radiotherapy treatment device is a linear accelerator.

6. A method of calibrating a radiotherapy treatment device comprising:

providing a source of radiation along an axis;

providing a dynamic phantom body formed of a material having a density proximally that of a human body;

providing a tank containing said dynamic phantom body;

providing at least one dosimetry probe constructed and arranged to sense photons and electrons;

positioning said at least one dosimetry probe within said dynamic phantom body;

supporting said dynamic phantom body and said tank on a carriage;

securing said carriage to a guideway;

incrementally moving said carriage, said tank and said dynamic phantom body relative to said guideway in a X-axis, a Y-axis and a Z-axis, said X-axis, said Y-axis and said Z-axis are substantially orthogonal to each other;

incrementally moving said at least one dosimetry probe with in said dynamic body relative to said tank; and

employing a controller to simultaneously move both said tank and said at least one dosimetry probe relative to each other to maintain the distance between a radiation source and the axis of a beam emitted from the radiation source to said at least one dosimetry probe constant;

whereby movement of said dynamic phantom body through a series of locations is carried out so as to provide sufficient data to determine the proper dose of radiation required for radiotherapy treatment.

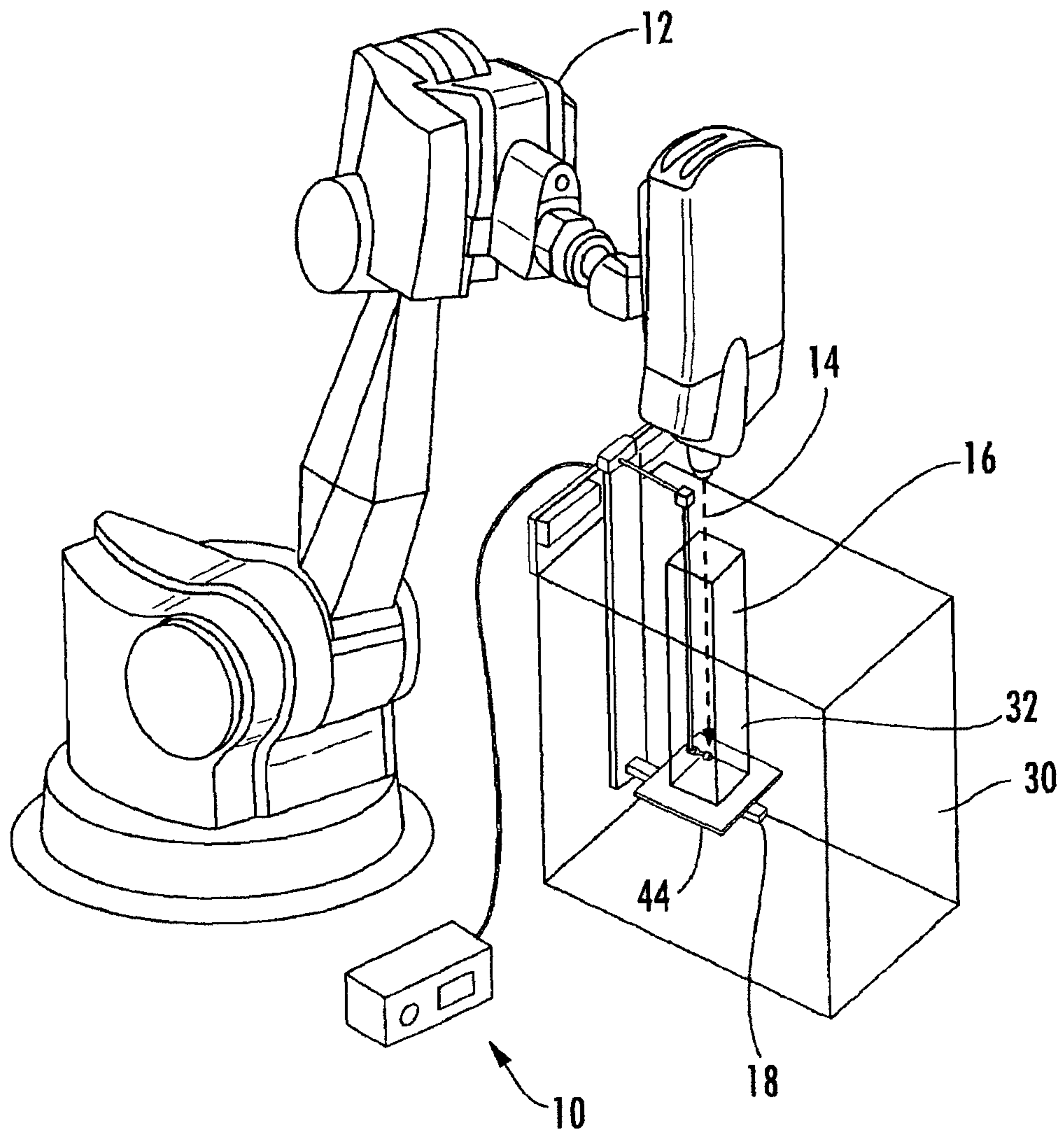


FIG. 1

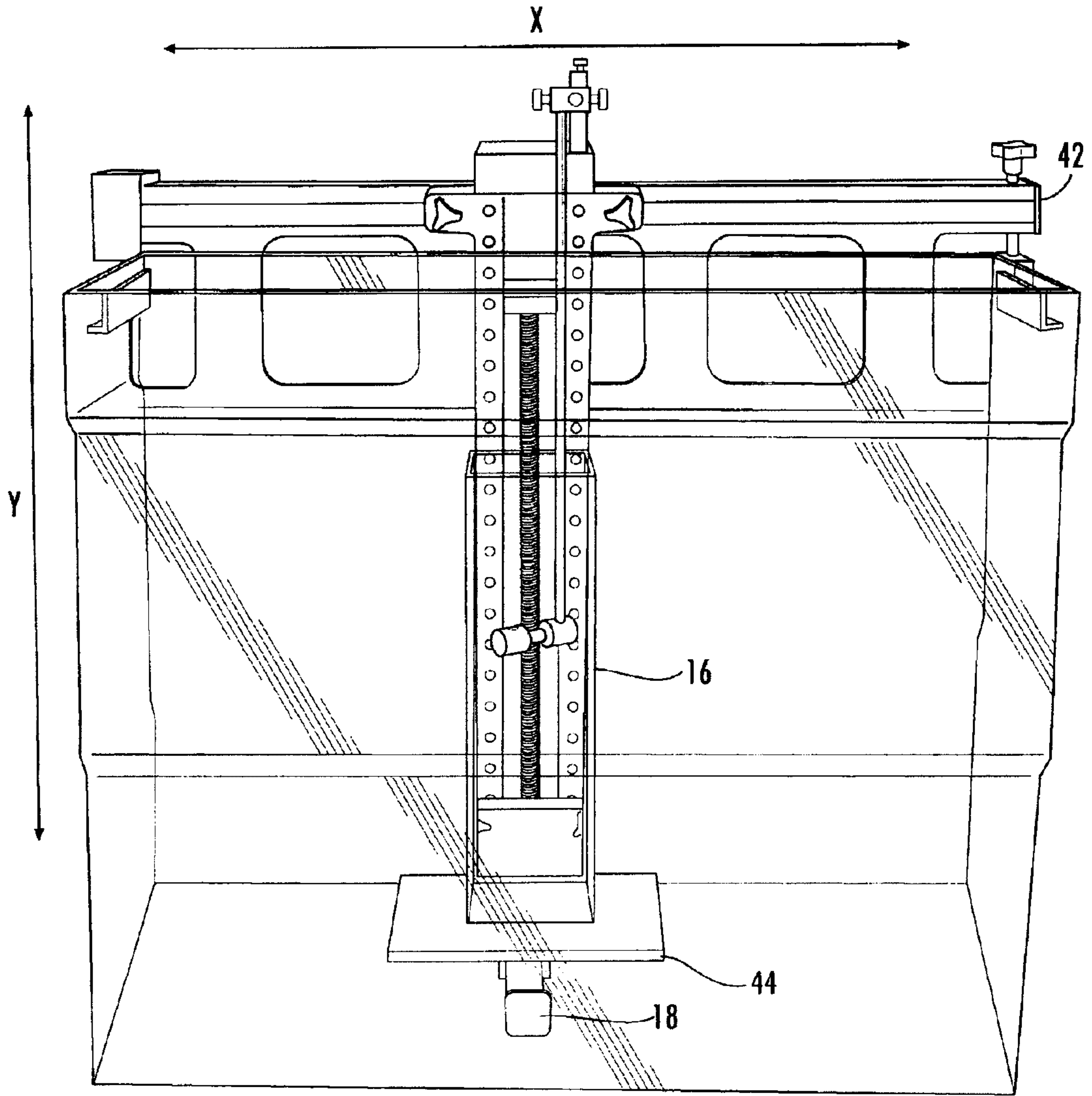


FIG. 2

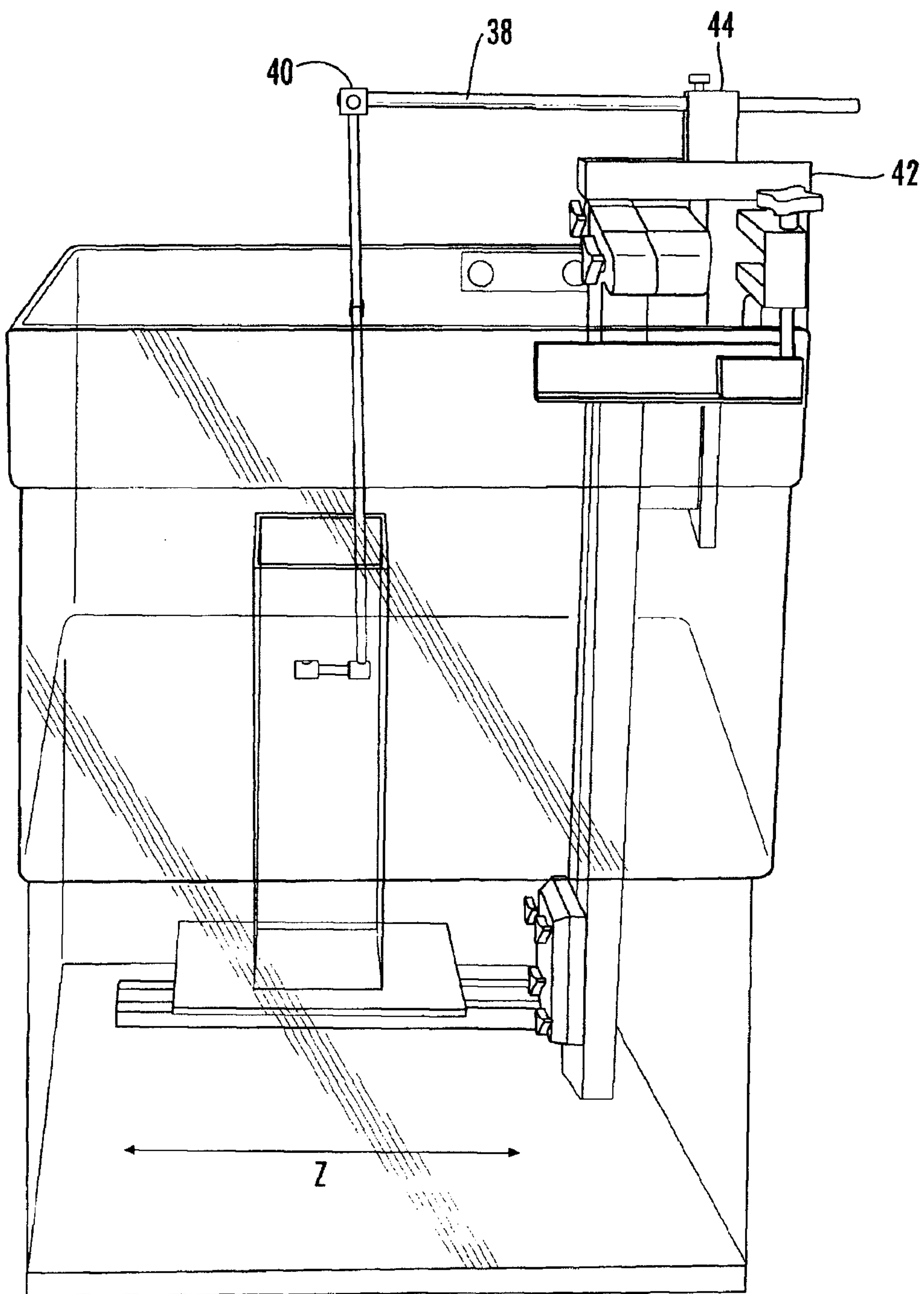


FIG. 3

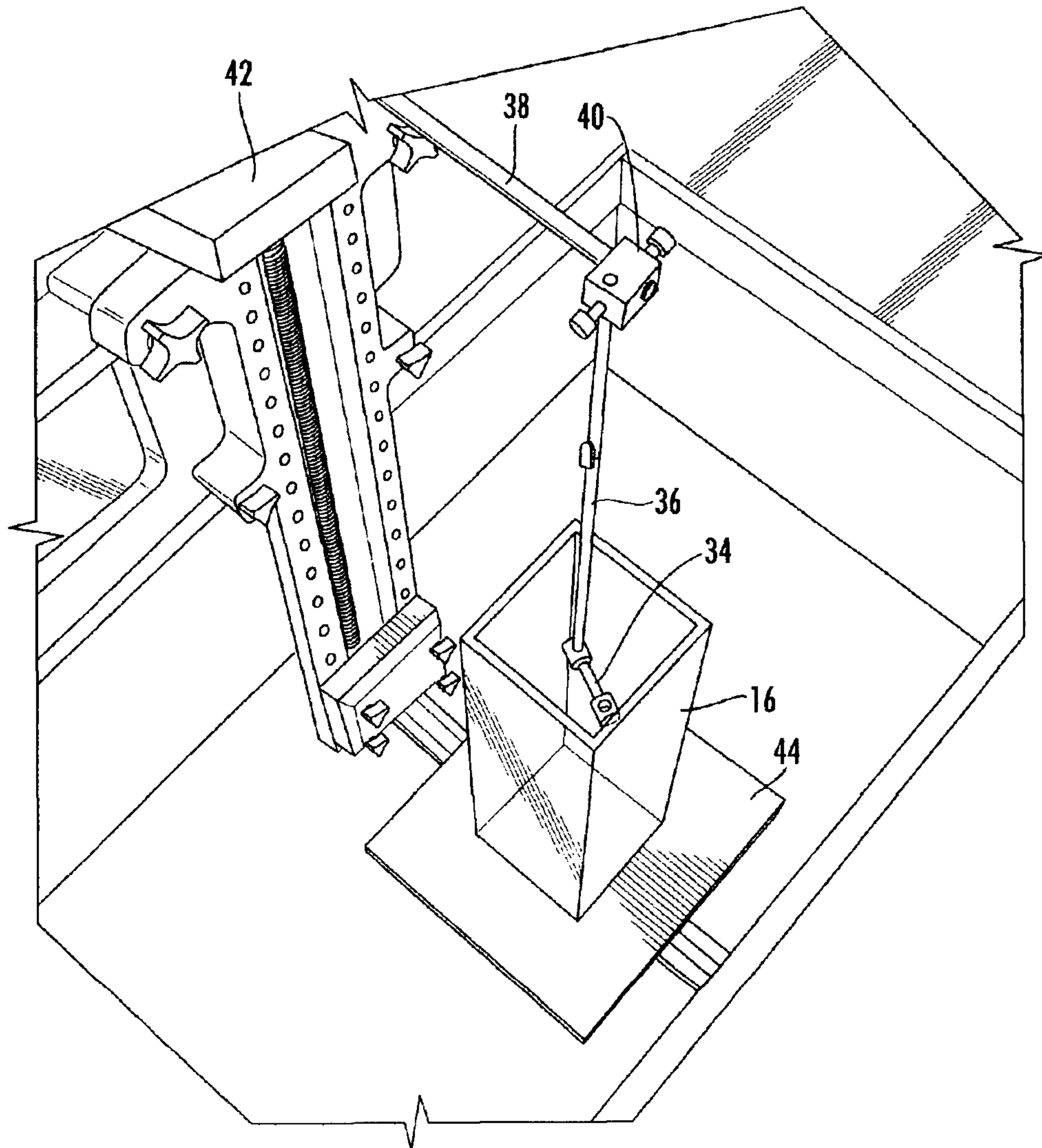
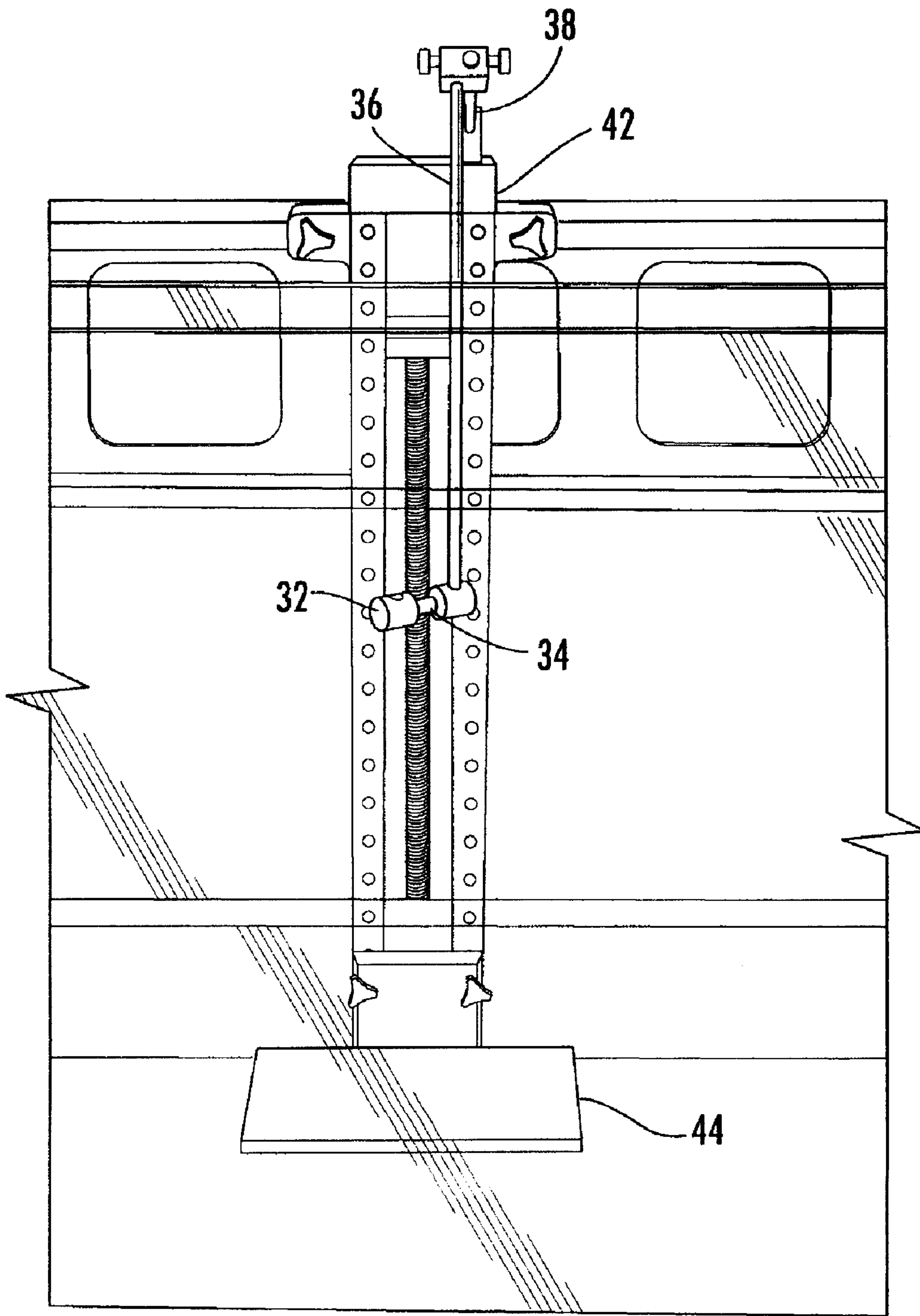


FIG. 4



**FIG. 5**

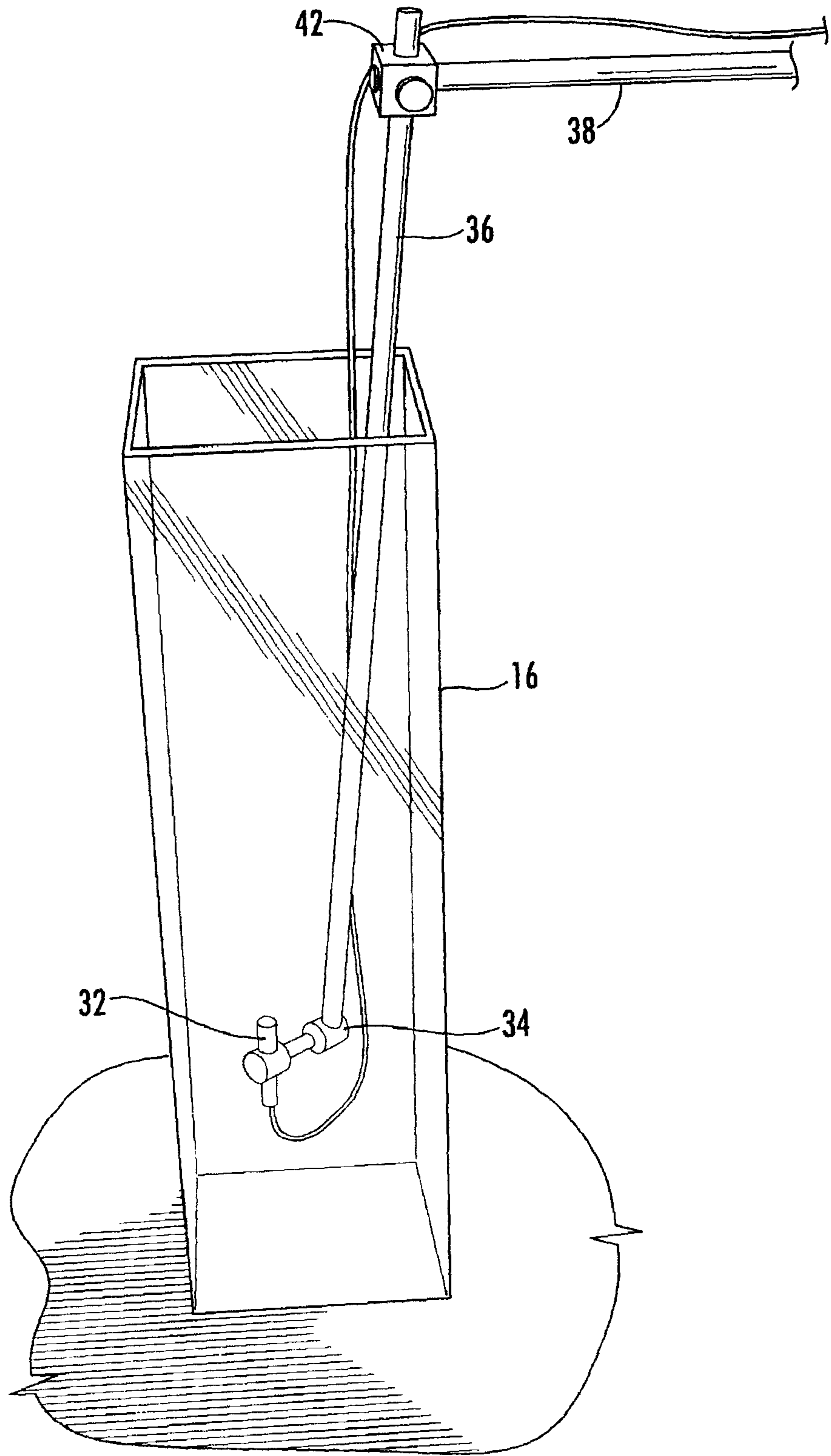
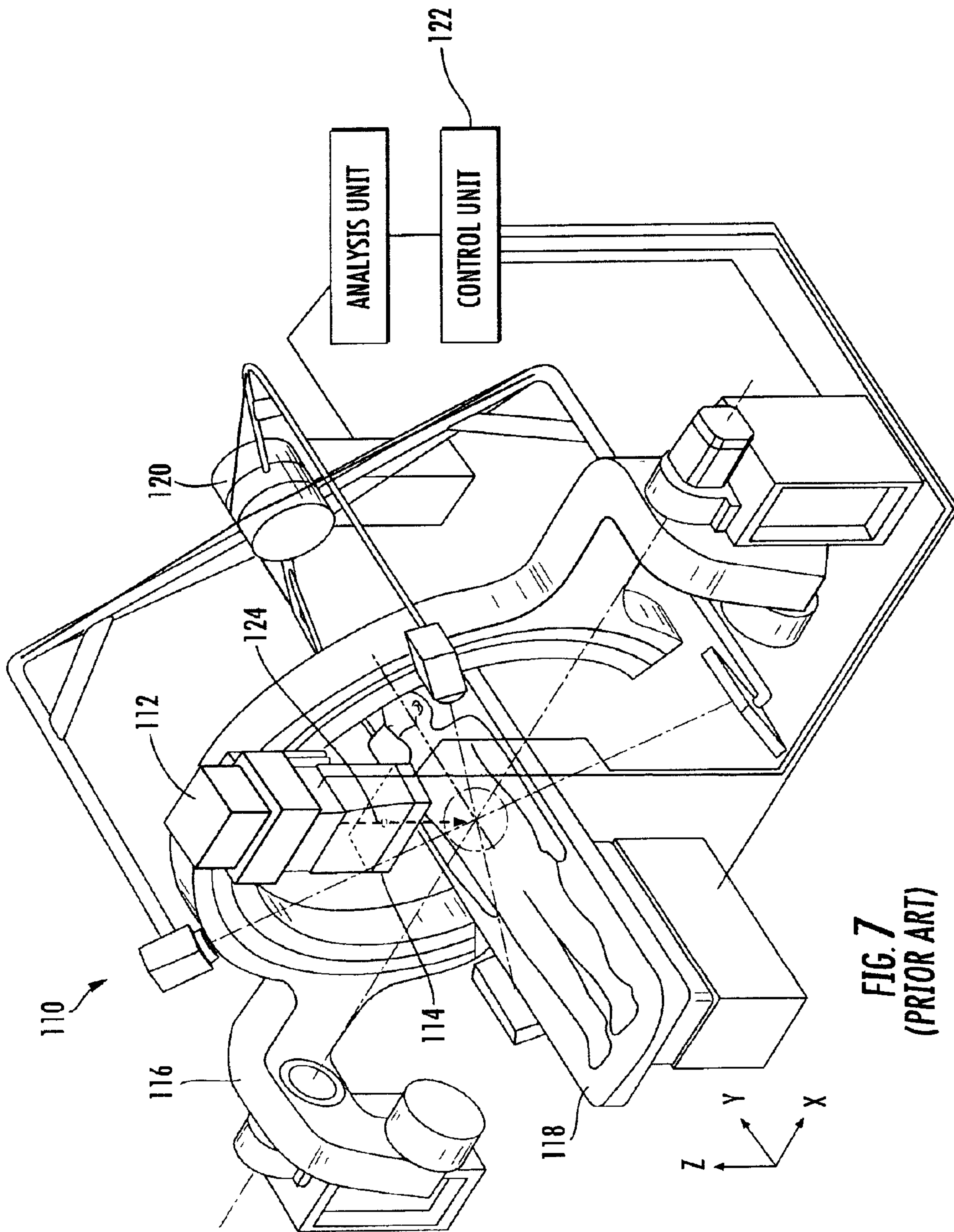


FIG. 6



**FIG. 7**  
**(PRIOR ART)**

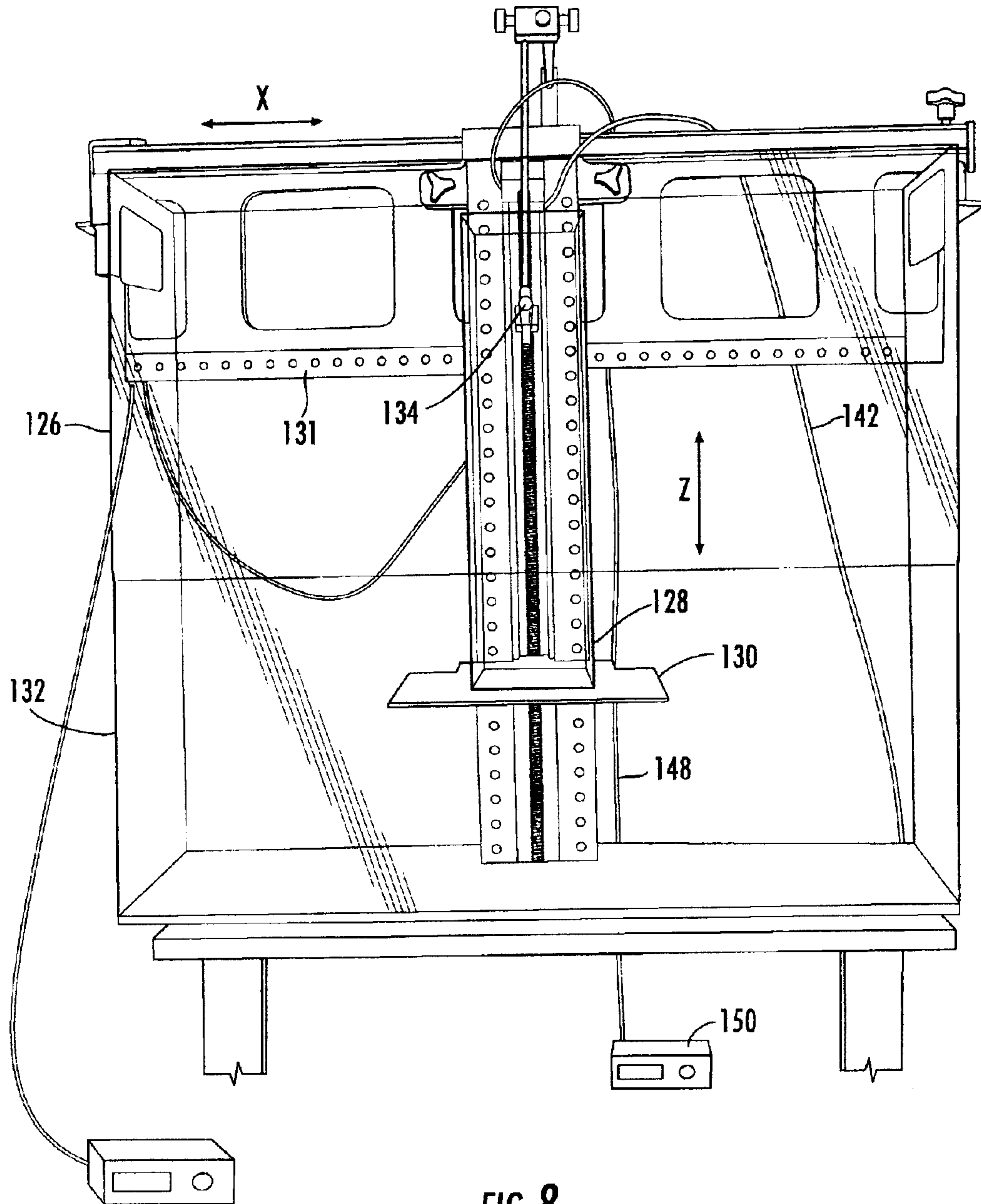


FIG. 8

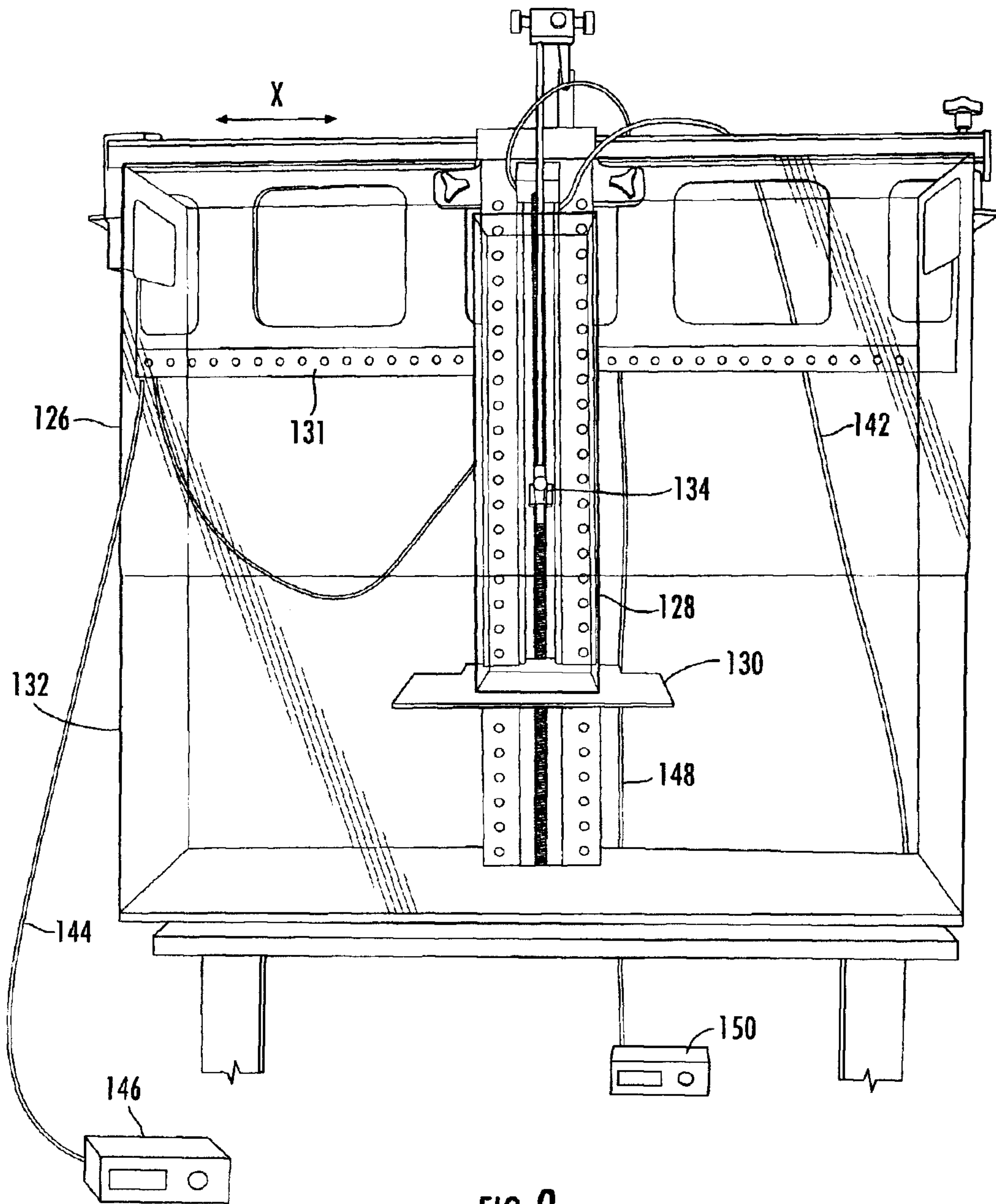
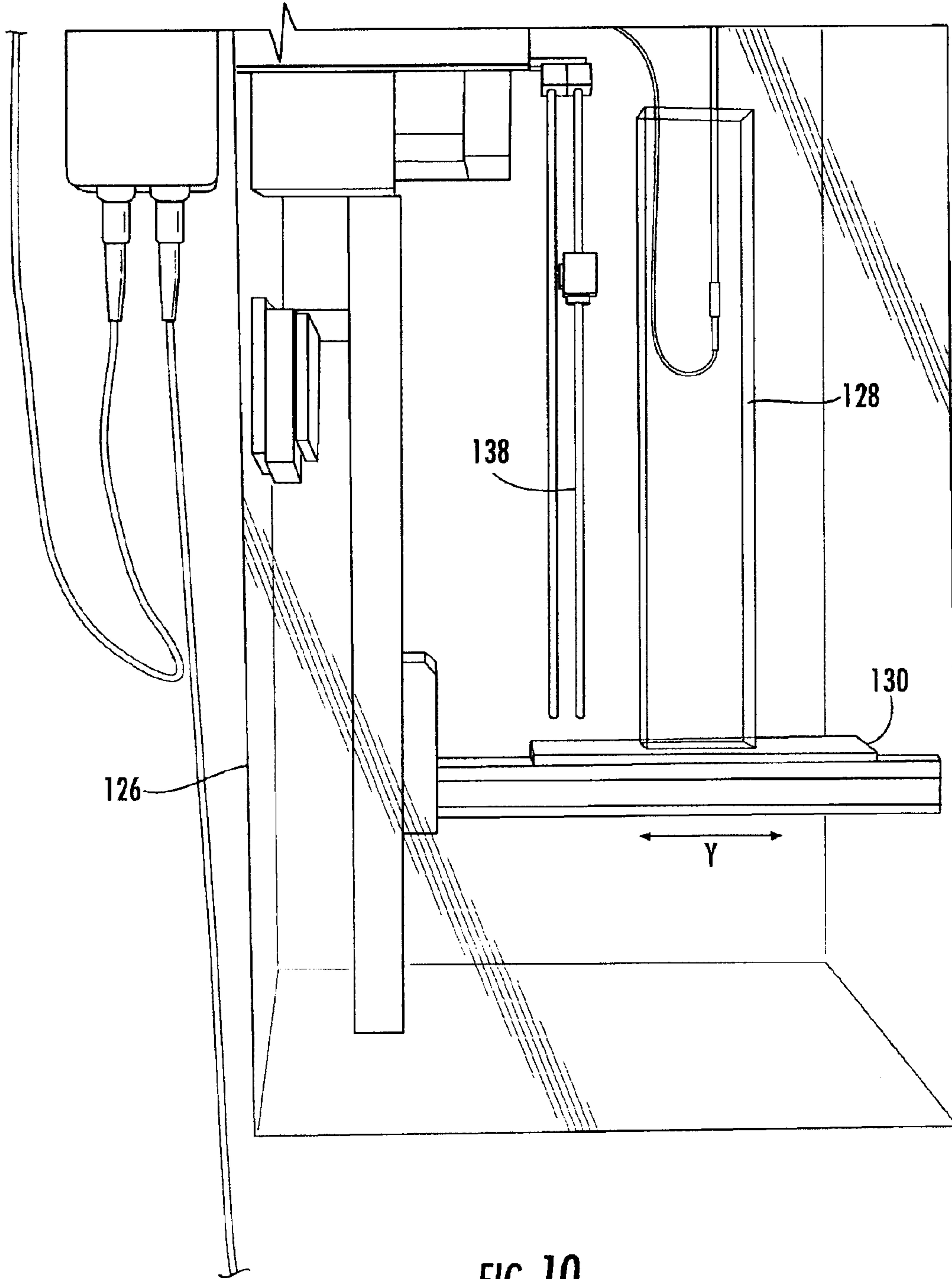
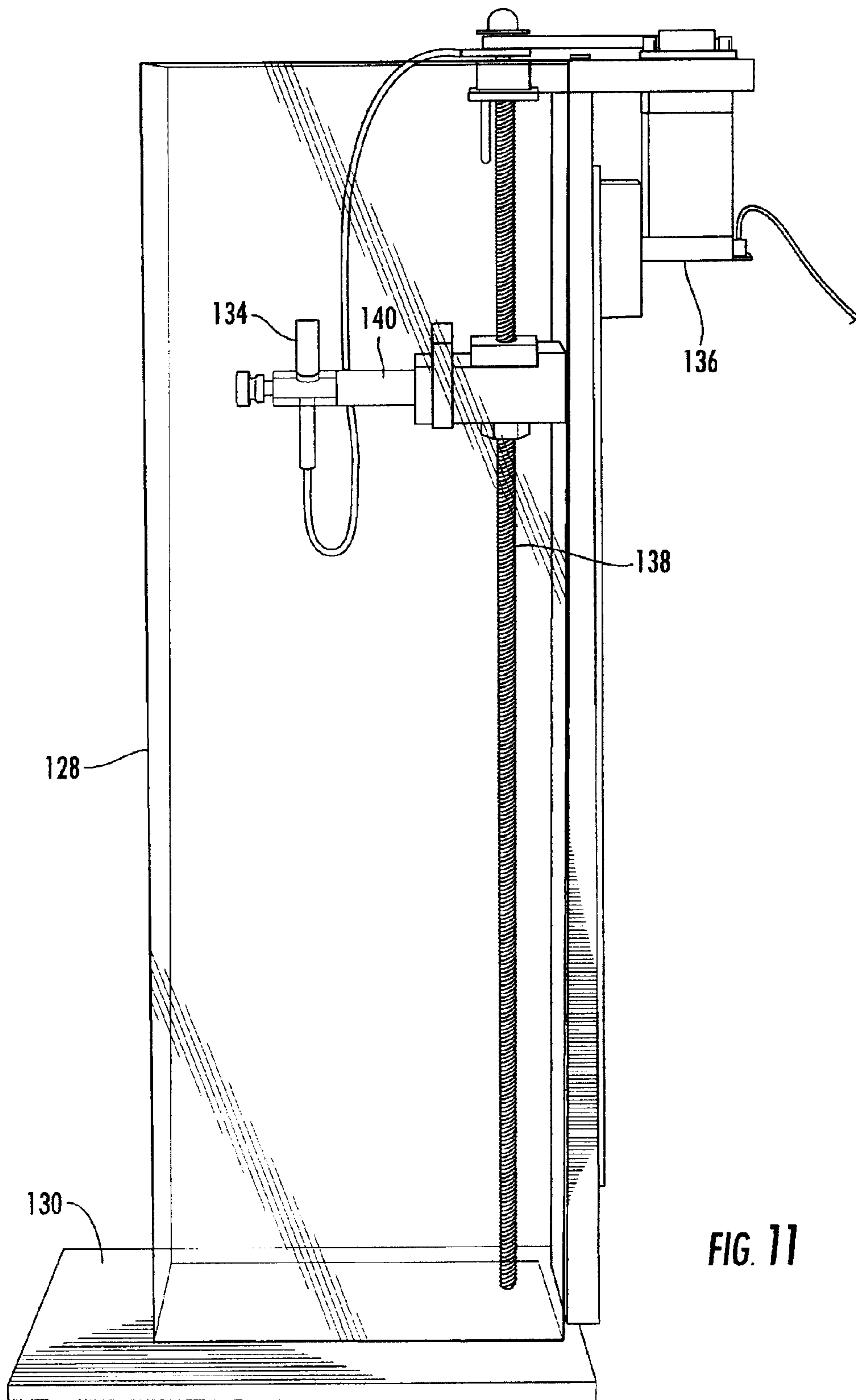


FIG. 9



**FIG. 10**



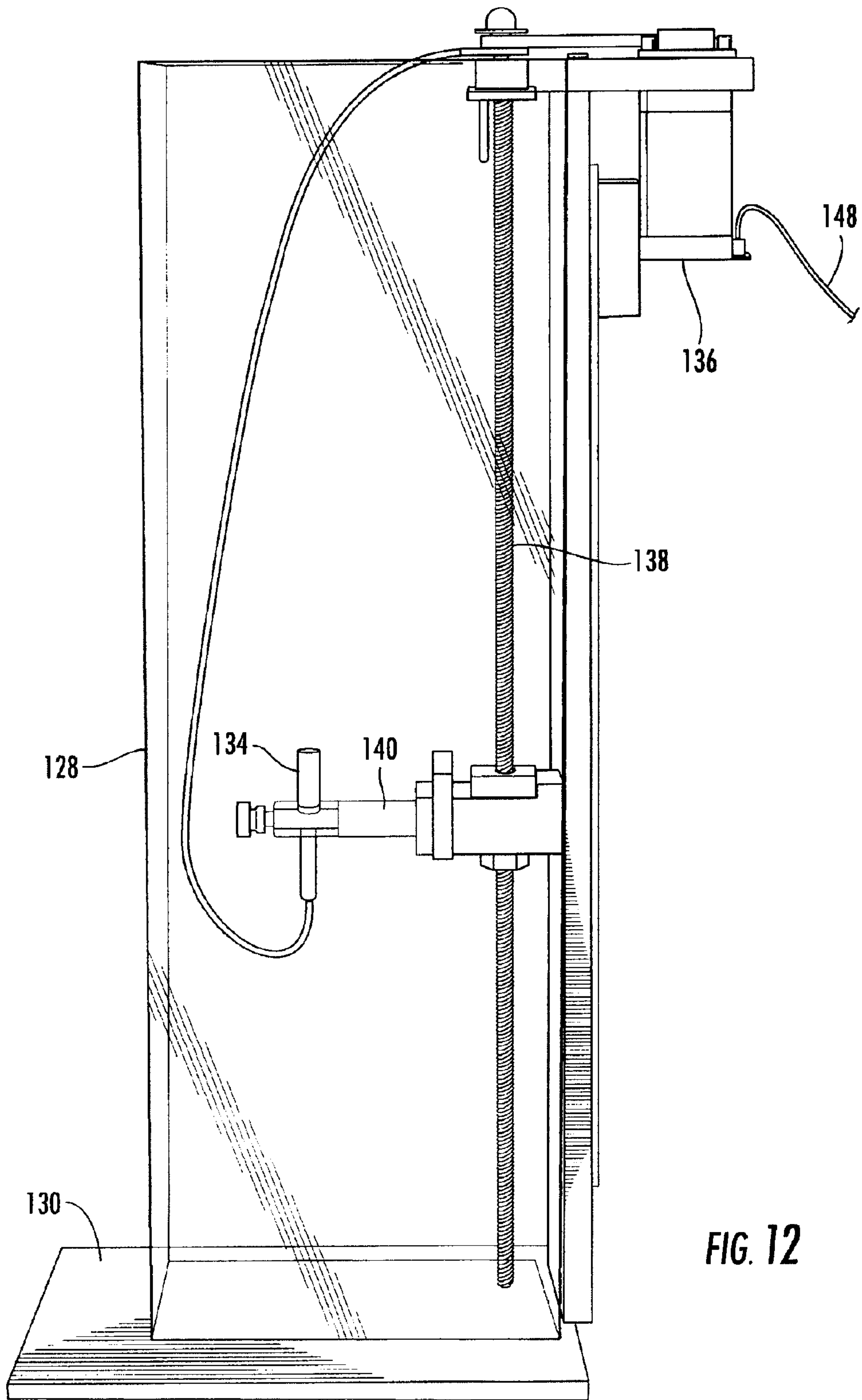


FIG. 12

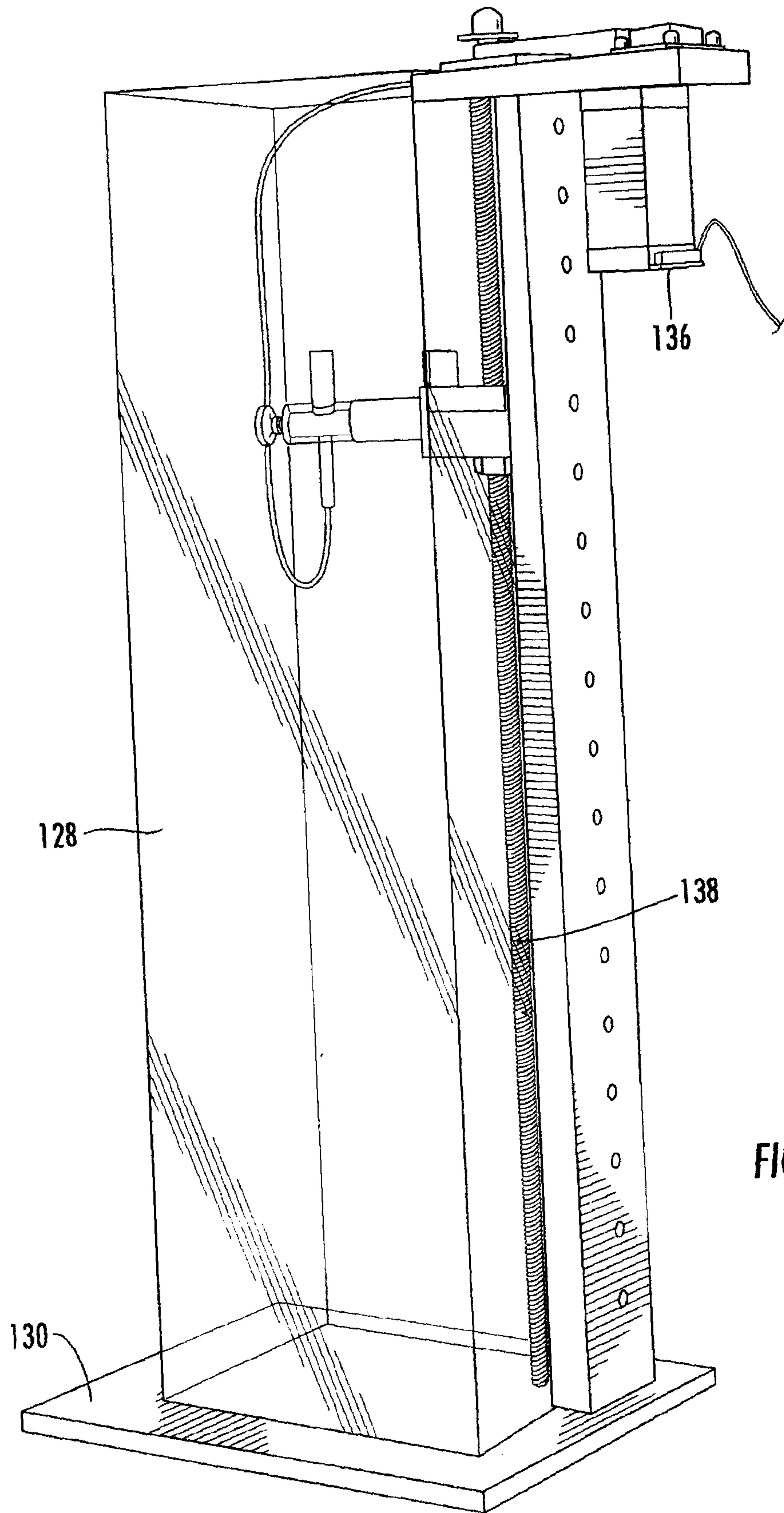


FIG. 13

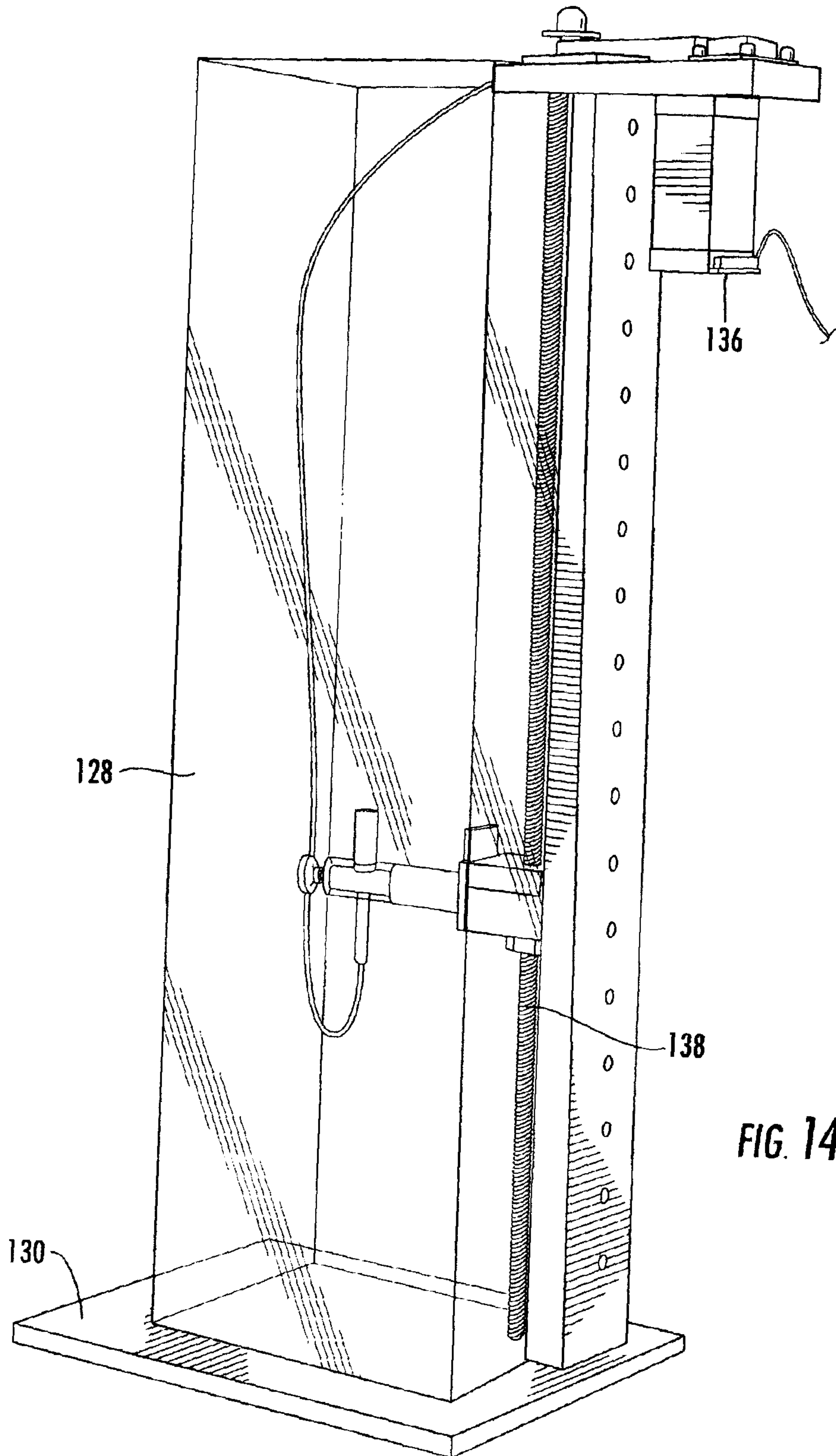


FIG. 14

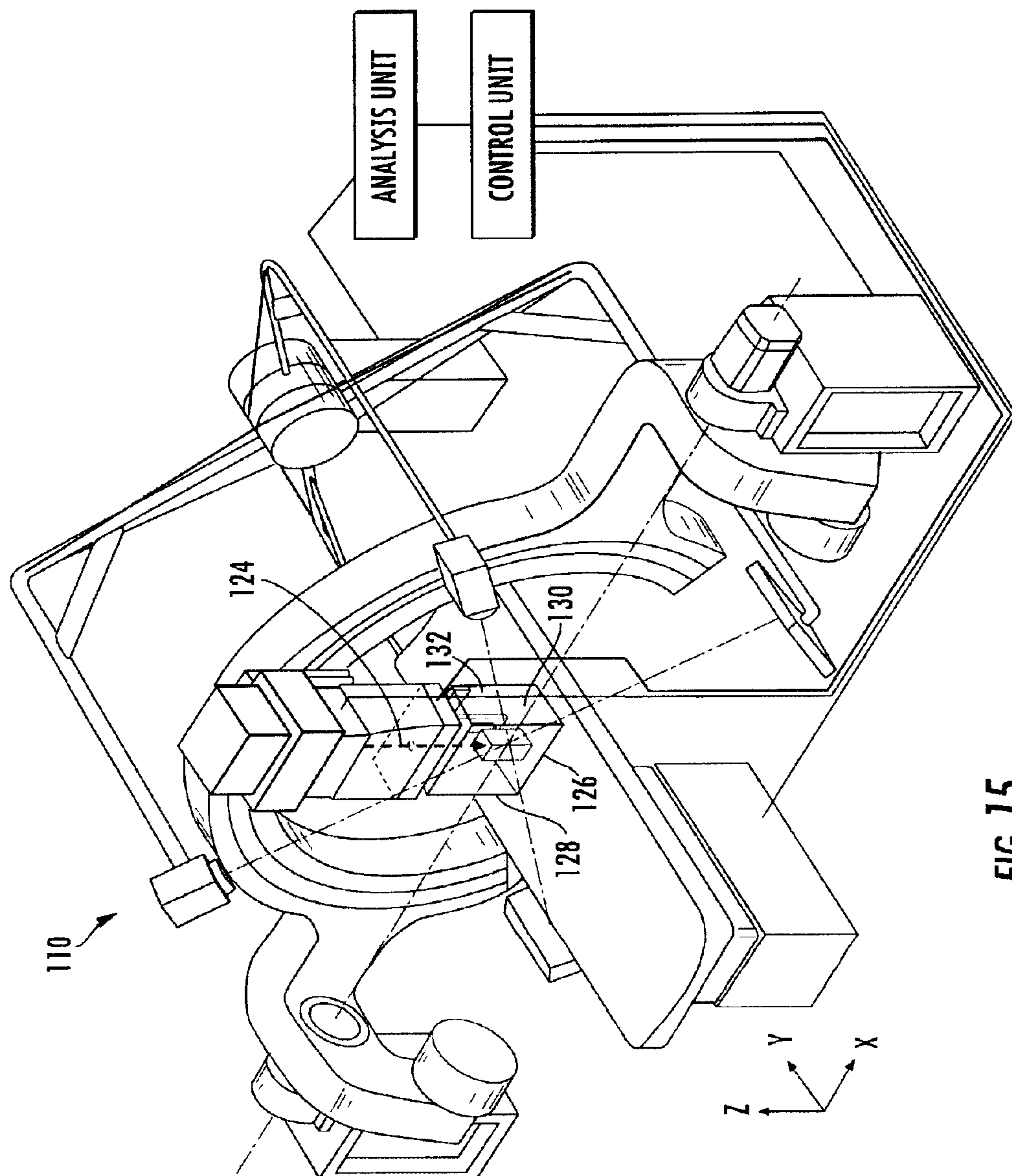


FIG. 15

CYBERKNIFE BEAM: 6cm DIAMETER

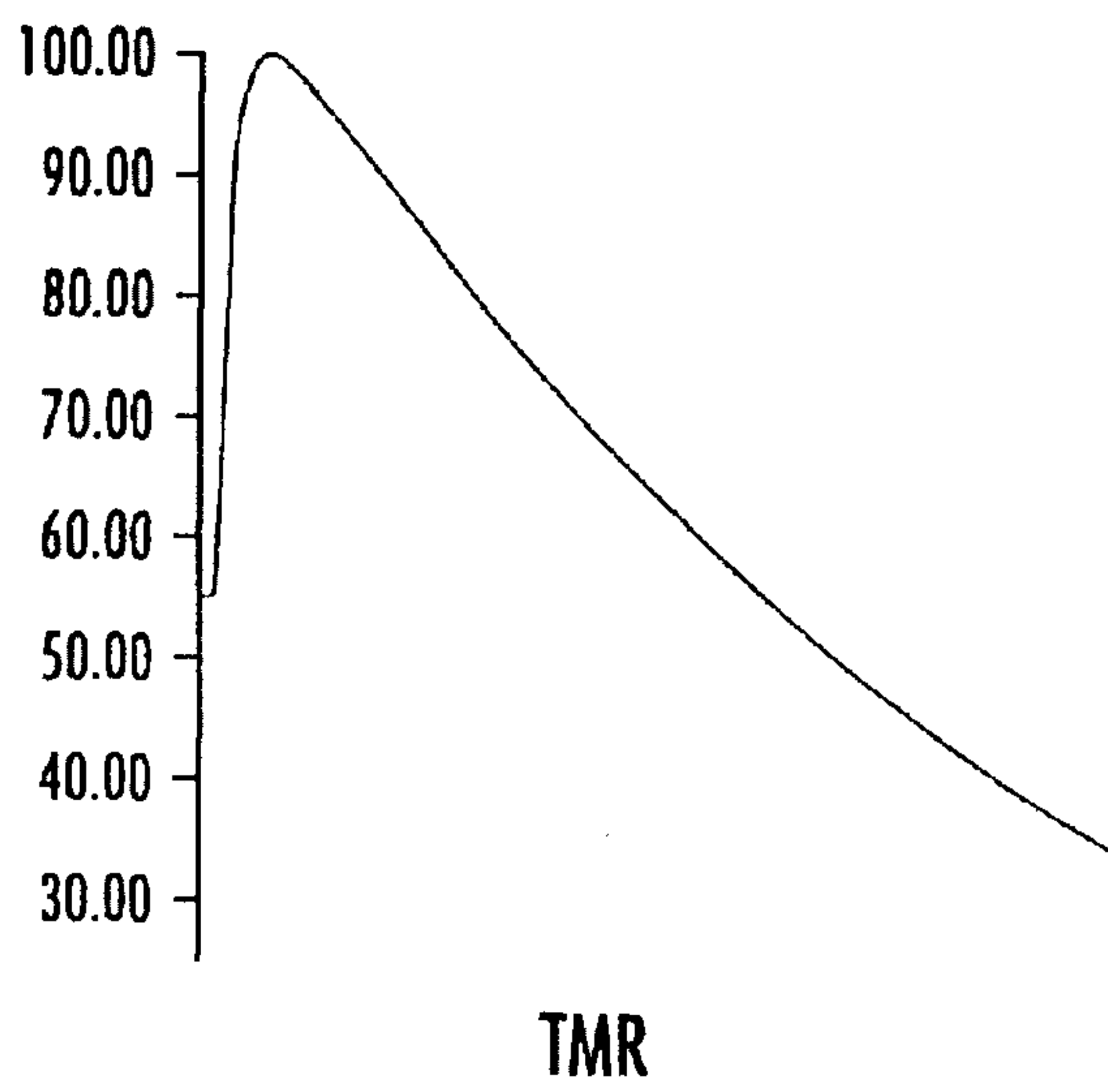


FIG. 16A

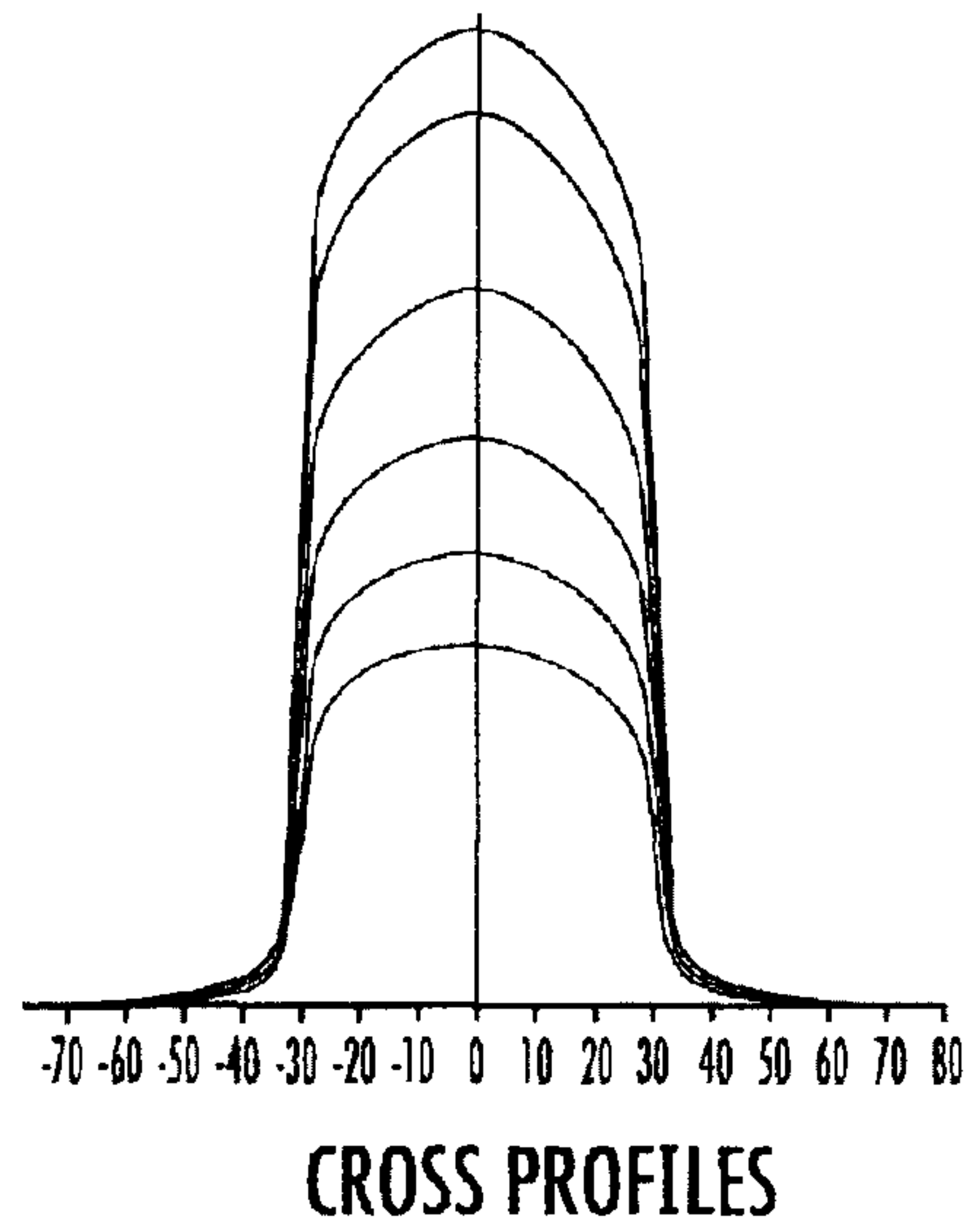


FIG. 16B

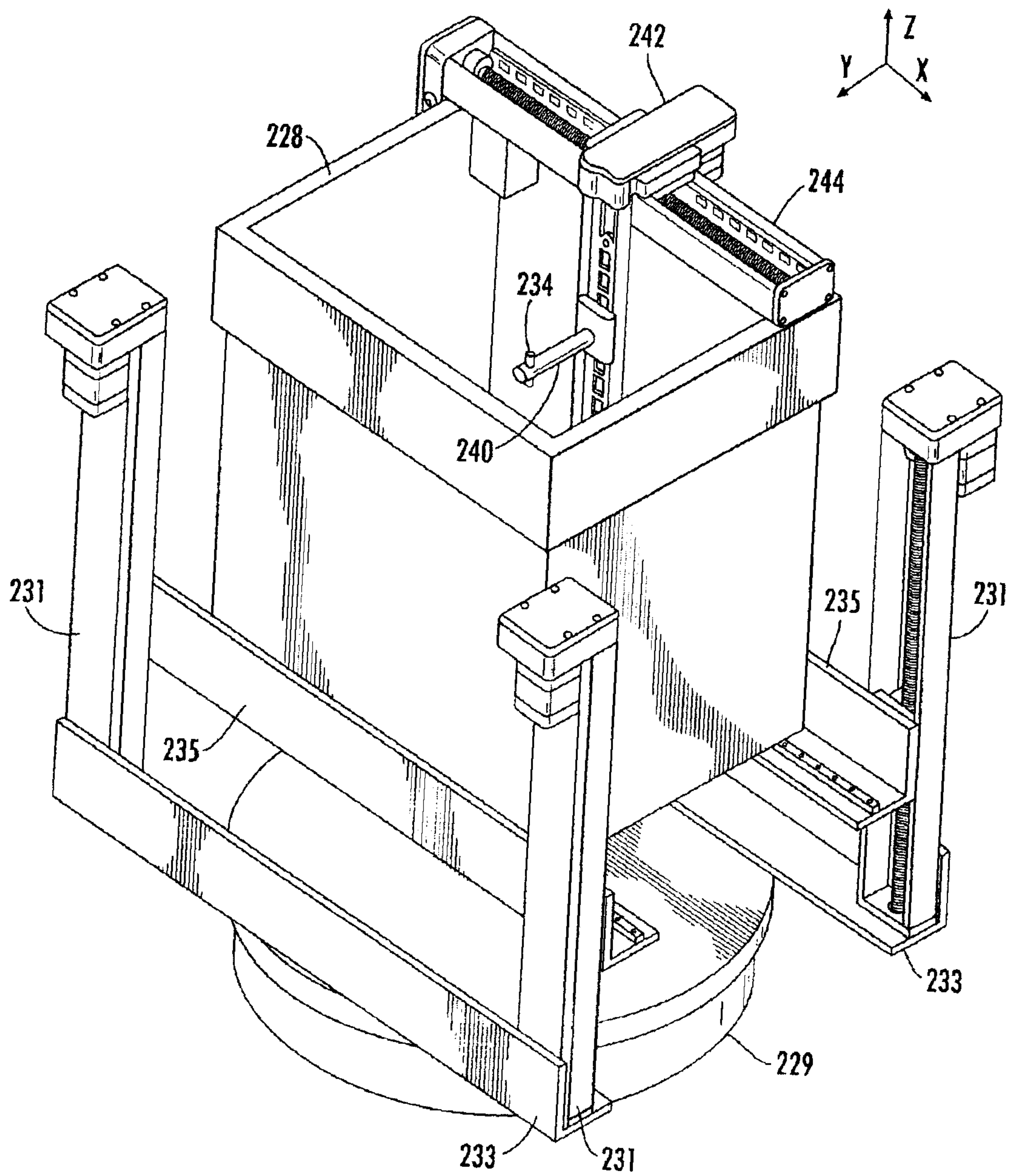
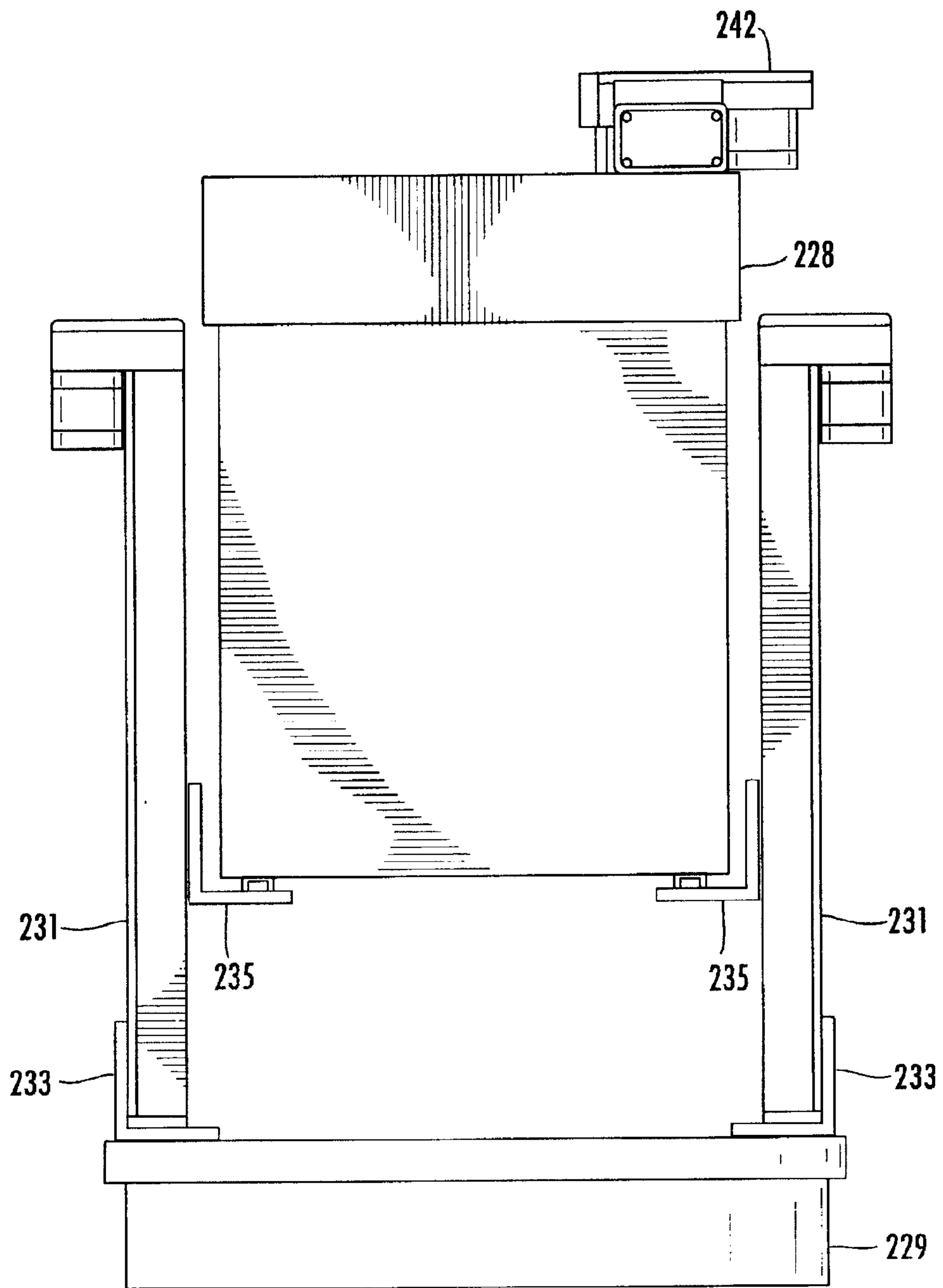


FIG. 17



**FIG. 18**

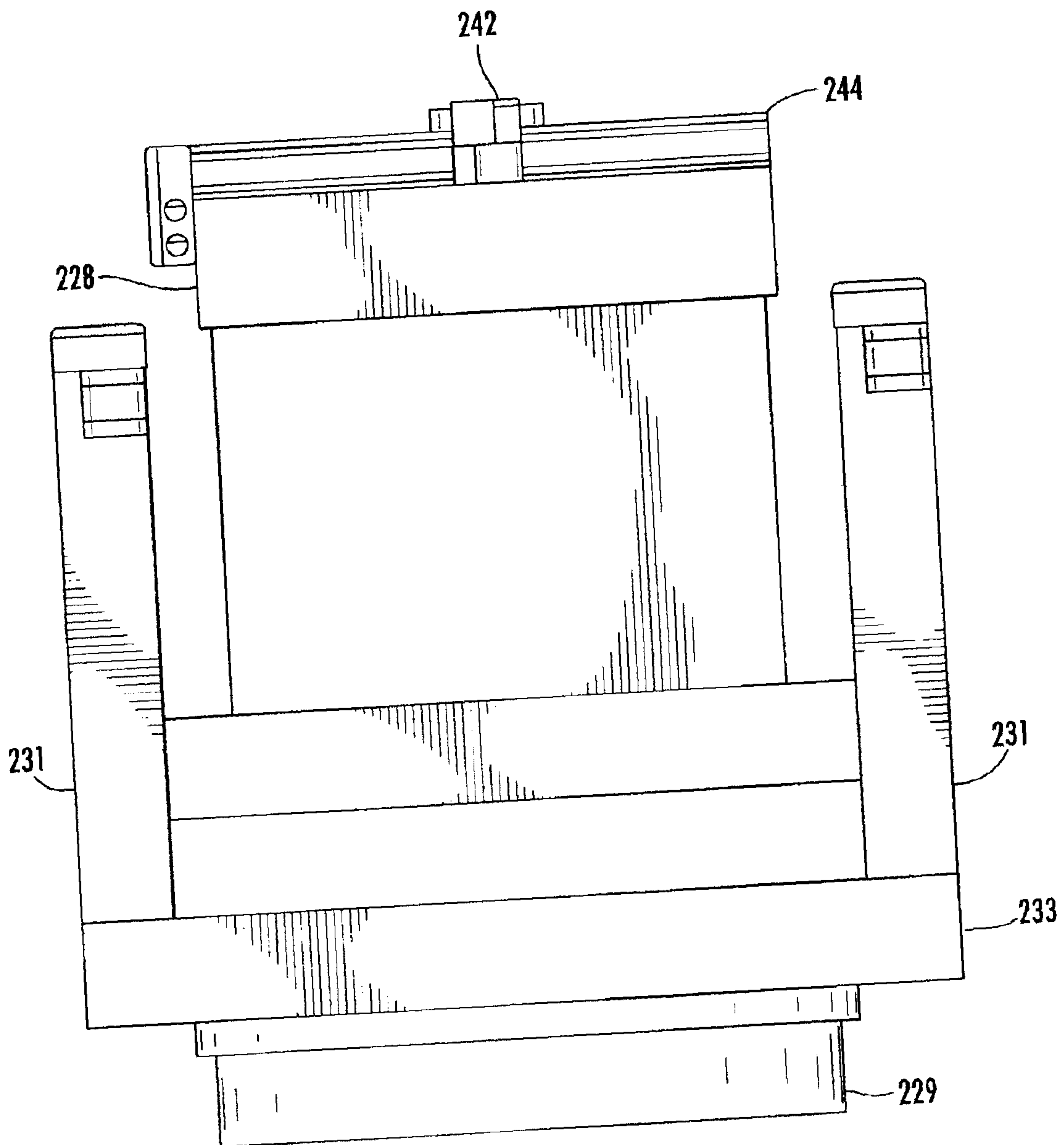


FIG. 19

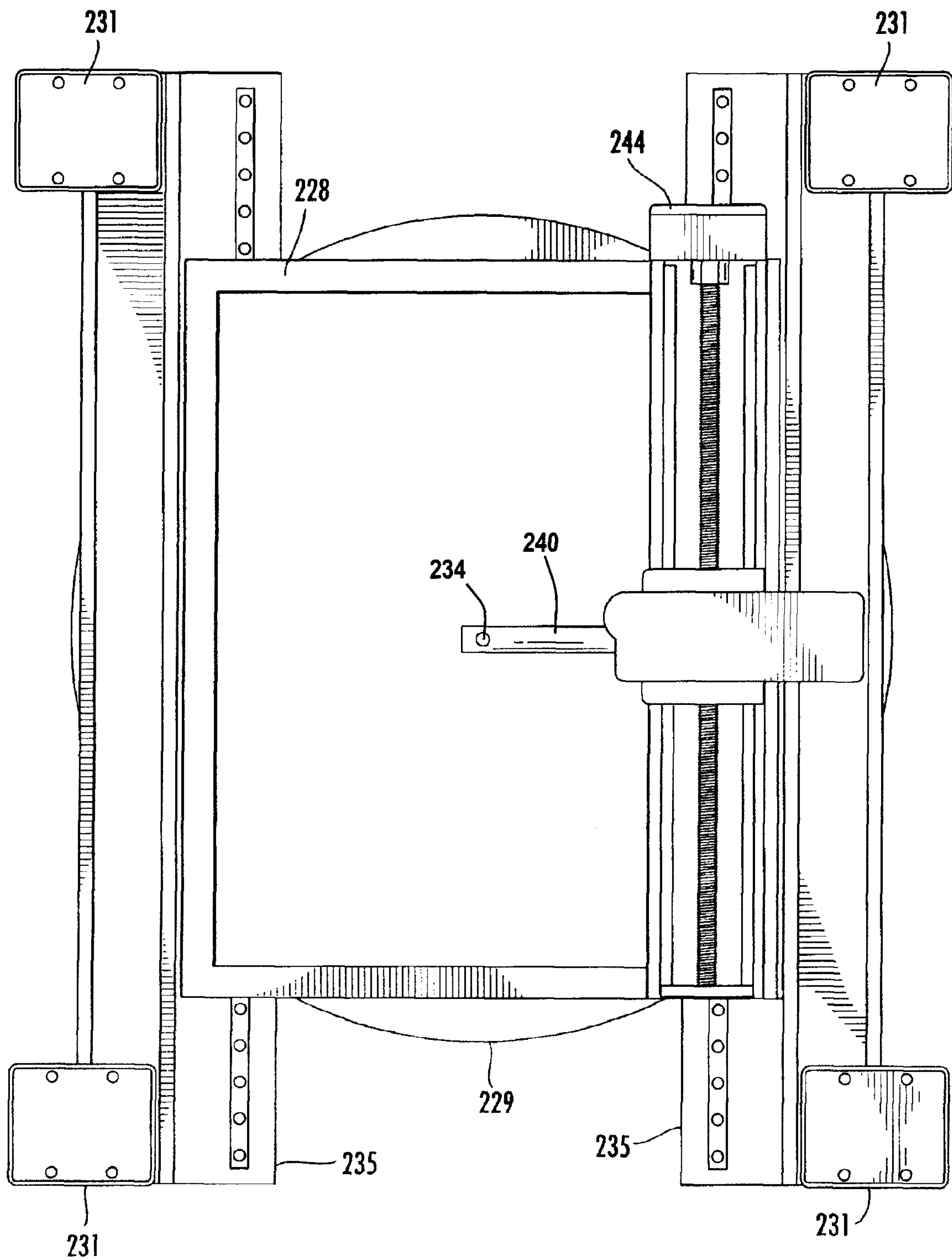


FIG. 20

