

(19) World Intellectual Property  
Organization  
International Bureau



(43) International Publication Date  
15 September 2005 (15.09.2005)

PCT

(10) International Publication Number  
**WO 2005/084638 A2**

(51) International Patent Classification<sup>7</sup>: **A61K 9/00**

(21) International Application Number:  
PCT/US2005/006903

(22) International Filing Date: 3 March 2005 (03.03.2005)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:  
60/550,601 5 March 2004 (05.03.2004) US  
60/560,470 7 April 2004 (07.04.2004) US  
60/564,189 21 April 2004 (21.04.2004) US  
60/572,631 19 May 2004 (19.05.2004) US  
60/579,425 14 June 2004 (14.06.2004) US  
10/990,996 17 November 2004 (17.11.2004) US

(71) Applicant (for all designated States except US): **PULMA-TRIX, INC.** [US/US]; 840 Memorial Drive, 3rd Floor, Cambridge, MA 02139 (US).

(72) Inventors; and

(75) Inventors/Applicants (for US only): **EDWARDS, David, A.** [US/US]; 171 Commonwealth Avenue, Boston, MA 02116 (US). **MAN, Jonathan, C.** [US/US]; 10 Rollins Court, Cambridge, MA 02139 (US). **KATSTRA, Jeffrey, P.** [US/US]; 40 Keith Street, Watertown, MA 02472 (US). **CLARKE, Robert, W.** [US/US]; 65 Morton Street, Canton, MA 02021 (US).

(74) Agents: **PABST, Patrea, L.** et al.; Pabst Patent Group LLP, 1201 Peachtree Street, Suite 1200, Atlanta, GA 30361 (US).

(81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SM, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.

(84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IS, IT, LT, LU, MC, NL, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

— without international search report and to be republished upon receipt of that report

For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

(54) Title: FORMULATIONS DECREASING PARTICLE EXHALATION

(57) Abstract: Formulations have been developed for pulmonary delivery to treat or reduce the infectivity of diseases such as viral infections, especially tuberculosis, SARS, influenza and respiratory syncytial virus in humans and hoof and mouth disease in animals, or to reduce the symptoms of allergy or other pulmonary disease. Formulations for pulmonary administration include a material that significantly alters physical properties such as surface tension and surface elasticity of lung mucus lining fluid, which may be isotonic saline and, optionally, a carrier. The formulation may be administered as a liquid solution, suspension, aerosol, or powder where the particles consist basically of an osmotically active solute. Drugs, especially antivirals or antibiotics, may optionally be included with the formulation. These may be administered with or incorporated into the formulation.



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## FORMULATIONS DECREASING PARTICLE EXHALATION

### Cross-Reference to Related Applications

This application claims priority to U.S. provisional application serial no. 60/579,425, filed June 14, 2004; U.S. provisional application serial no. 60/572,631, filed May 19, 2004; U.S. provisional application serial no. 60/564,189, filed April 21, 2004; U.S. provisional application serial no. 60/560,470, filed April 7, 2004; U.S. provisional application serial no. 60/550,601, filed March 5, 2004, and U.S. utility application serial no. 10/990,996, filed November 17, 2004.

### Field of the Invention

The present invention is in the field of formulations and systems to decrease the incidence of bioaerosol exhalation.

### Background of the Invention

Viral and bacterial infections are frequently highly contagious, especially when spread by respiration. The recent reports regarding Severe Acute Respiratory Syndrome ("SARS"), now known to be caused by a corona virus, are proof of how rapidly an infection can spread when it is transmitted through air contact. Other diseases such as influenza spread by air contact, and rapidly reach epidemic proportions, with high numbers of fatalities in elderly and immunocompromised populations.

SARS is a respiratory illness that has recently been reported in Asia, North America, and Europe. As of April 20, 2003, about 198 suspect cases of SARS and 38 probable cases of SARS had been reported in the United States. In general, SARS begins with a fever greater than 100.4°F [ $>38.0^{\circ}\text{C}$ ]. Other symptoms may include headache, an overall feeling of discomfort, and body aches. Some people also experience mild respiratory symptoms. After 2 to 7 days, SARS patients may develop a dry cough and have trouble breathing.

SARS appears to spread primarily by close person-to-person contact. Most SARS cases have involved people who cared for or lived with someone with SARS, or had direct contact with infectious material (for example, respiratory secretions) from a person who has SARS. Potential ways in

which SARS can be spread include touching the skin of other people or objects that are contaminated with infectious droplets and then touching your eye(s), nose, or mouth. This can happen when someone who is sick with SARS coughs or sneezes droplets onto themselves, other people, or nearby  
5 surfaces. It is also possible that SARS can be spread more broadly through the air or by other ways that are currently not known. At present there is no treatment or means of prevention for SARS, other than supportive care.

TB, or tuberculosis, is a disease caused by the bacteria *Mycobacterium tuberculosis*. The bacteria can attack any part of the body,  
10 but usually attacks the lungs. TB was once the leading cause of death in the United States. In the 1940s, scientists discovered the first of several drugs now used to treat TB. As a result, TB slowly began to disappear in the United States. Recently, TB has made a resurgence. Between 1985 and 1992, the number of TB cases increased, with more than 16,000 cases  
15 reported in the United States in 2000 alone.

TB is spread through the air from one person to another. The bacteria are dispersed into the air when a person with TB of the lungs or throat coughs or sneezes. People nearby may breathe in these bacteria and become infected.  
20 When a person breathes in *Mycobacterium tuberculosis*, the bacteria can settle in the lungs and begin to grow. From there, it can spread through the blood to other parts of the body, such as the kidney, spine, and brain. People with TB are most likely to spread it to people they come in contact with on a daily basis. People who are infected with latent TB do not feel sick, are  
25 asymptomatic, and cannot spread TB, but they may develop TB at some time in the future. Bacteria are not the only sources of infectious diseases. Viruses are also highly contagious and have no effective treatments other than containment. For example, Respiratory syncytial virus (RSV) is a very common virus that causes mild cold-like symptoms in adults and older  
30 healthy children. By age two, nearly all infants have been infected by RSV. RSV can cause severe respiratory infections in infants, particularly those born prematurely, with heart or lung disease, or immunocompromised.

Seasonal outbreaks of acute respiratory illness typically occur in the fall and last into the spring. RSV is spread easily by physical contact. Transmission is usually by contact with contaminated secretions, called foamites, which may involve tiny droplets or objects that droplets have touched. RSV can live for half an hour or more on human hands. The virus can also live up to five hours on countertops and for several hours on used tissues. RSV often spreads very rapidly in crowded households and day care centers. Each year up to 125,000 infants are hospitalized due to severe RSV disease, and about 1-2% of these infants die. It has been reported that exogenous surfactant supplementation in infants with respiratory syncytial virus bronchiolitis was beneficial (Tibby, et al. Am J Respir Crit Care Med 2000 Oct; 162(4 Pt 1):1251). The principle means of treatment remains supportive however, and there is no means of limiting spread other than isolation.

Influenza is another common viral infection for which there is no effective treatment, and containment is the only option to limit spread of disease. Influenza is caused by three viruses - Influenza A, B and C. Type A is usually responsible for large outbreaks and is most adept at mutating. New strains of Type A virus develop regularly and cause new epidemics every few years. Type B causes smaller outbreaks, and Type C usually causes mild illness. In the United States, infection with influenza A and B leads to 20,000 deaths and over 100,000 hospitalizations each year. Influenza is transmitted person to person via contagious droplets that are formed when someone sneezes or coughs. Approximately 8 million children and adolescents between 6 months and 17 years of age have one or more medical conditions that put them at increased risk of influenza-related complications. Such children include those with chronic disorders of the heart or lungs (such as asthma and cystic fibrosis), children who have required regular medical follow-up or hospitalization during the preceding year because of chronic metabolic diseases (including diabetes mellitus), kidney dysfunction, sickle cell anemia, or immunosuppression.

For unvaccinated individuals who have been exposed to people with known influenza, especially if the exposed individual has risk factors,

potential use of antiviral medication for more than 2 weeks and vaccination may help prevent illness. For mild illness in people who are not at high-risk, the treatment of influenza is frequently just supportive and includes bed rest, analgesics for muscle aches and pains, and increased intake of fluids.

5 Treatment is usually not necessary for children, but may be prescribed if the illness is diagnosed early and the patient is at risk of progression to more severe infection. Among individuals in high-risk groups (elderly, immunosuppressed, chronic heart, lung or kidney conditions) influenza may be quite severe and can lead to complications or death.

10 Epidemics of respiratory infections are not limited to humans. Foot-and-mouth disease virus (FMDV) is the etiologic agent of foot-and-mouth disease (FMD), which is a disease of cattle, swine, and other cloven-footed animals. FMD is characterized by the formation of vesicles on the tongue, nose, muzzle, and coronary bands of infected animals. Several unique  
15 characteristics make the virus one of the most economically devastating diseases in the world today. The ease with which it may be transmitted by contact and aerosol, combined with its enhanced ability to initiate infections, virtually ensures that most, if not all, animals in a herd will contract FMD. The long-term survival of FMDV in infected animals' tissues and organs,  
20 especially when refrigerated, offers an opportunity for its national and international transmission through the food chain. Multiple serotypes and numerous subtypes reduce the effectiveness and reliability of vaccines. The possible development of carriers in vaccinated animals and those that have recovered from FMD provides additional potential sources of new outbreaks.  
25 These features create a disease that can have a major economic impact on live stock operations around the world. The foot and mouth disease (FMD) epidemic in British livestock remains an ongoing cause for concern, with new cases still arising in previously unaffected areas (Ferguson, et al., *Nature* 2001 414(6861):329). The parameter estimates obtained in a  
30 dynamic model of disease spreading show that extended culling programs were essential for controlling the epidemic to the extent achieved, but

demonstrate that the epidemic could have been substantially reduced in scale had the most efficient methods been used earlier in the outbreak.

Viral shedding through bioaerosol exhalation is one mechanism, for infection transmission from a host leading to inhalation by another animal or human. The devastating consequences that uncontrolled viral shedding can have on livestock were seen in the hoof and mouth disease outbreak in the U.K., where 2030 confirmed cases resulted in the mandatory slaughter of 4 million animals. Recently, more attention is being given to the threat of bioterrorism and the similar risk that a sudden outbreak of disease poses to livestock in the U.S.

Airborne infection is one of the main routes of pathogen transmission. Aerosols composed of mucus droplets originating in the lungs and nasal cavities are produced when a human or animal coughs or simply breathes. These bioaerosols can contain pathogens that transmit the disease upon inhalation by exposed humans or animals. In addition, respirable pathogenic bioaerosols produced in the upper airways can be re-breathed by the host leading to parenchymal infection with exacerbated disease outcomes.

WO03/092654 to David Edwards *et al.* describes a method for diminishing the spread of inhaled infections by delivering materials such as surfactants that suppress bioaerosol expiration. This technique works on the basis of altering the surface or other physical properties of the endogenous surfactant fluid in the lungs, and thereby favoring fewer exhaled bioaerosol particles. It would be desirable to have other means of limiting bioaerosol formation and/or spread.

It is therefore an object of the present invention to provide formulations for use in decreasing or limiting spread of pulmonary infections, especially viral or bacterial infections, without delivery of surfactant material to the lungs.

It is further an object of the present invention to provide a method of treatment to decrease or limit the spread of pulmonary infections to other animals or humans, especially viral or bacterial infections.

It is further an object of the present invention to provide a method of treatment to decrease or limit the spread of pulmonary infections, especially viral or bacterial infections, within a patient.

It is further an object of the present invention to provide formulations  
5 for treatment of humans or animals to limit infectivity.

It is yet a further object of this invention to manufacture a device for the measurement of exhaled particle number and particle size to diagnose those animals or humans with an enhanced propensity to exhale aerosols.

### Summary of the Invention

10 Formulations have been developed for delivery by any route to reduce the infectivity of diseases such as viral infections, especially tuberculosis, SARS, influenza, cytomegalovirus and RSV in humans and hoof and mouth disease in animals. In one embodiment, the formulation for administration is a non-surfactant solution that, via dilution of endogenous  
15 surfactant fluid, alters physical properties such as surface tension, surface elasticity and bulk viscosity of lung mucus lining fluid. The aerosolized material may be an isotonic saline solution, a hypertonic saline solution or other solution containing osmotically active materials. The formulation may be administered as a powder where the particles consist essentially of a salt  
20 or osmotically-active substance that dilutes endogenous surfactant fluid. The aerosol may be a solution, suspension, spray, mist, vapor, droplets, particles, or a dry powder, for example, using a metered dose inhaler including HFA propellant, a metered dose inhaler with non-HFA propellant, a nebulizer, a pressurized can, or a continuous sprayer. The aerosol is preferably an  
25 aqueous solution, and more preferably isotonic saline, or it may contain a particularly effective osmotically-active substance, like mannitol. The formulation may be an organic suspension or solution for aerosol delivery. The formulation may be a vapor. Typical concentrations of salts or sugars are in the range of up to 5 or 6% solute. In a preferred embodiment, the  
30 formulations are administered either as a powder or aerosol, preferably prior to or shortly after infection, allergy or asthma attack. The formulations are administered to decrease or prevent exhalation of particulate matter,

especially of infectious particulate matter. The formulation is administered in an amount sufficient to decrease surface instabilities in the liquid lining the airways of the lung, i.e., to damp the rate of droplet formation from lung fluid, without causing expectoration. Examples demonstrate suitable  
5 formulations and effective amounts. An example demonstrates efficacy of administration of nebulized saline over a period of up to twelve minutes, preferably two minutes or greater, to decrease particle exhalation in cattle.

A method of screening animals or humans for a number of characteristics, including the measurement of expired air and inspired air, the  
10 assessment of exhaled particle numbers, the assessment of exhaled particle size and the assessment of tidal volume and respiratory frequency during sampling, was devised to aid in the diagnosis of animals or humans who have an enhanced propensity to exhale aerosols. A device with sufficient sensitivity to accurately count sub-micron sized particles was designed and  
15 assembled. The device is portable and operates on batteries. Particle number and size can be determined by infrared spectroscopy, laser diffraction or light scattering.

#### **Brief Description of the Drawings**

Figure 1 is a diagram of the simulated cough machine apparatus.  
20 Figure 2 illustrates an actual cough profile versus a simulated cough profile.

Figure 3 illustrates particle concentration following three coughs measured over time for plain mucus simulant and following saline delivery at  $t=0$ ,  $t=30$  and  $t=60$  minutes.

25 Figure 4A is a chart of baseline particle count (greater than 150nm) expired by individuals ( $n=11$ ) while inhaling particle free air; and Figure 4B is a graph of particle count (greater than 150nm) expired by individuals ( $n=11$ ) after saline (approximately 1g) had been administered to the lungs in the form of an aerosol over time (minutes).

30 Figure 5A is a graph of particle count (greater than 150 nm) exhaled by individuals ( $n=2$ ) who, prior to treatment have a baseline exhalation of greater than 1000 particles/liter (while inhaling particle free air), after



isotonic saline solution (approximately 1g solution) had been administered to the lungs in the form of an aerosol over time (minutes); and Figure 5B is a graph of particle count (greater than 150 nm) exhaled by individuals (n=2) who, prior to treatment have a baseline exhalation of greater than 1000 particles/liter (while inhaling particle free air), after isotonic saline solution containing phospholipids (approximately 1g solution) had been administered to the lungs in the form of an aerosol over time (minutes).

Figure 6A is a graph of total particles exhaled (greater than 0.3 microns) over time (minutes) showing data obtained from sham treated animals. Figure 8B is a graph of mean percent (%) baseline particle counts over time (minutes) showing data obtained from animals treated with nebulized saline for 1.8 minutes (-■-), 6.0 minutes (-▲-), 12.0 minutes (-□-), and sham (-◆-).

### Detailed Description of the Invention

Lung mucociliary clearance is the primary mechanism by which the airways are kept clean from particles present in the liquid film that coats them. The conducting airways are lined with ciliated epithelium that beat to drive a layer of mucus towards the larynx, clearing the airways from the lowest ciliated region in 24 hours. The fluid coating consists of water, sugars, proteins, glycoproteins, and lipids. It is generated in the airway epithelium and the submucosal glands, and the thickness of the layer ranges from several microns in the trachea to approximately 1 micron in the distal airways in humans, rat, and guinea pig.

A second important mechanism for keeping the lungs clean is via momentum transfer from the air flowing through the lungs to the mucus coating. Coughing increases this momentum transfer and is used by the body to aid the removal of excess mucus. It becomes important when mucus cannot be adequately removed by ciliary beating alone, as occurs in mucus hypersecretion associated with many disease states. Air speeds as high as 200 m/s can be generated during a forceful cough. The onset of unstable sinusoidal disturbances at the mucus layer has been observed at such air speeds. This disturbance results in enhanced momentum transfer from the

air to the mucus and consequently accelerates the rate of mucus clearance from the lungs. Experiments have shown that this disturbance is initiated when the air speed exceeds some critical value that is a function of film thickness, surface tension, and viscosity (M. Gad-El-Hak, R.F. Blackwelder, J.J. Riley. *J. Fluid Mech.* – (1984) 140:257-280). Theoretical predictions and experiments with mucus-like films suggest that the critical speed to initiate wave disturbances in the lungs is in the range of 5-30 m/s.

Papineni and Rosenthal (*J. Aerosol Med.*, 1997, 10(2): 105-116) have demonstrated that during standard mouth and nose breathing, or during coughing, normal human subjects expire tens to hundreds of liquid bioaerosol droplets, with a preponderance of exhaled bioaerosol droplets having a diameter smaller than one micron. Coughing was shown to give rise to the greatest number of particles, although the mean exhaled particle size remained significantly less than a micron. The majority of these particles are larger than most inhaled pathogens, i.e., greater than 150 nm. For instance, some common inhaled pathogens have characteristic sizes in this range: tuberculosis, 1,000-5,000 nm; influenza, 80-120 nm; measles, 100-250 nm; chicken pox, 120-200 nm; FMD, 27-30 nm.

## **I. Formulations**

Bioaerosol particles are formed by instabilities in the endogenous surfactant layer in the airways. This instability depends on endogenous surfactant concentration in the lungs. This surfactant concentration can be altered by simply diluting the endogenous surfactant pool via either delivery of isotonic saline (though not in such a large amount as to cause a subject to expectorate) or a hypertonic saline solution that causes the cells lining the lung's airways to dilute further the endogenous surfactant layer via production of water.

The formulations described herein are effective to decrease aerosol exhalation, by preventing or reducing exhaled particle formation from the oropharynx or nasal cavities. A preferred aerosol solution for altering physical properties of the lung's lining fluid is isotonic saline. Saline

solutions have long been delivered chronically to the lungs with small amounts of therapeutically active agents, such as beta agonists, corticosteroids, or antibiotics. For example, VENTOLIN<sup>®</sup> Inhalation Solution (GSK) is an albuterol sulfate solution used in the chronic treatment of asthma and exercise-induced bronchospasm symptoms. A VENTOLIN<sup>®</sup> solution for nebulization is prepared (by the patient) by mixing 1.25-2.5mg of albuterol sulfate (in 0.25-0.5mL of aqueous solution) into sterile normal saline to achieve a total volume of 3mL. No adverse effects are thought to be associated with the delivery of saline to the lungs by VENTOLIN<sup>®</sup> nebulization, even though nebulization times can range from 5-15 minutes. Saline is also delivered in more significant amounts to induce expectoration. Often these saline solutions are hypertonic (sodium chloride concentrations greater than 0.9%, often as high as 5%) and generally they are delivered for up to 20 minutes.

It has been discovered that physical properties of the endogenous surfactant fluid in the lungs, such as surface tension, can be altered by administration of a saline solution, as well as by administration of an aqueous saline solution containing other materials, such as surfactant.

The term "aerosol" as used herein refers to any preparation of a fine mist of particles, typically less than 10 microns in diameter, which can be in solution or a suspension. The preferred mean diameter for aqueous formulation aerosol particles is about 3 microns, for example between 0.1 and 30 microns, most preferably between 1 and 10 microns. The aerosol can consist just of a solution, such as an aqueous solution, most preferably a saline solution. Alternatively, the aerosol may consist of an aqueous suspension or dry particles. Concentration ranges of the salt or other osmotically active material range from about 0.01% to about 10% by weight, preferably between 0.9% to about 10%.

#### **A. Osmotically Active Materials**

Many materials may be osmotically active, including binary salts, such as sodium chloride, or any other kinds of salts, or sugars, such as mannitol. Osmotically active materials, normally owing to their ionization

and possibly size, do not easily permeate cell membranes and therefore exert an osmotic pressure on contiguous cells. Such osmotic pressure is essential to the physical environment of cellular material, and regulation of this pressure occurs by cell pumping of water into or out of the cell. Solutions delivered to the lungs that are isotonic normally do not create an imbalance in osmotic pressure in the lung fluid and therefore simply dilute the natural endogenous lung fluid with water and salt. Solutions of high osmotic content (i.e. hypertonic solutions) create an imbalance of osmotic pressure, with greater pressure in the lung fluid, causing cells to pump water into the lung fluid and therefore further dilute lung surfactant composition.

#### **B. Active Ingredients**

The formulations disclosed herein can be used by any route for delivery of a variety of molecules, especially antivirals and anti-infective molecules including antibiotics, antihistamines, bronchodilators, cough suppressants, anti-inflammatories, vaccines, adjuvants and expectorants. Examples of macromolecules include proteins and large peptides, polysaccharides and oligosaccharides, and DNA and RNA nucleic acid molecules and their analogs having therapeutic, prophylactic or diagnostic activities. Nucleic acid molecules include genes, antisense molecules that bind to complementary DNA to inhibit transcription, and ribozymes. Preferred agents are antiviral, steroid, bronchodilators, antibiotics, mucus production inhibitors and vaccines.

In the preferred embodiment, the concentration of the active agent ranges from about 0.01% to about 20% by weight. In a more preferred embodiment, the concentration of active agent ranges from between 0.9% to about 10%.

#### **II. Carriers and Aerosols for Administration**

Carriers can be divided into those for administration via solutions (liquid formulations) and those for administration via particles (dry powder formulations).

### A. Liquid Formulations

Aerosols for the delivery of therapeutic agents to the respiratory tract have been developed. See, for example, Adjei, A. and Garren, *J. Pharm. Res.*, 7: 565-569 (1990); and Zanen, P. and Lamm, J.-W. *J. Int. J. Pharm.*, 114: 111-115 (1995). These are typically formed by atomizing the solution or suspension under pressure through a nebulizer or through the use of a metered dose inhaler ("MDI"). In the preferred embodiment, these are aqueous solutions or suspensions.

### B. Dry Powder Formulations

The geometry of the airways is a major barrier for drug dispersal within the lungs. The lungs are designed to entrap particles of foreign matter that are breathed in, such as dust. There are three basic mechanisms of deposition: impaction, sedimentation, and Brownian motion (J.M. Padfield. 1987. In: D. Ganderton & T. Jones eds. *Drug Delivery to the Respiratory Tract*, Ellis Harwood, Chichester, U.K.). Impaction occurs when particles are unable to stay within the air stream, particularly at airway branches. They are adsorbed onto the mucus layer covering bronchial walls and cleaned out by mucocilliary action. Impaction mostly occurs with particles over 5  $\mu\text{m}$  in diameter. Smaller particles ( $<5 \mu\text{m}$ ) can stay within the air stream and be transported deep into the lungs. Sedimentation often occurs in the lower respiratory system where airflow is slower. Very small particles ( $<0.6 \mu\text{m}$ ) can deposit by Brownian motion. This regime is undesirable because deposition cannot be targeted to the alveoli (N. Worakul & J.R. Robinson. 2002. In: *Polymeric Biomaterials*, 2<sup>nd</sup> ed. S. Dumitriu ed. Marcel Dekker. New York).

The preferred mean diameter for aerodynamically light particles for inhalation is at least about 5 microns, for example between about 5 and 30 microns, most preferably between 3 and 7 microns in diameter. The particles may be fabricated with the appropriate material, surface roughness, diameter and tap density for localized delivery to selected regions of the respiratory tract such as the deep lung or upper airways. For example, higher density or larger particles may be used for upper airway delivery. Similarly, a mixture

of different sized particles, provided with the same or different therapeutic agent may be administered to target different regions of the lung in one administration.

As used herein, the phrase "aerodynamically light particles" refers to particles having a mean or tap density less than about  $0.4 \text{ g/cm}^3$ . The tap density of particles of a dry powder may be obtained by the standard USP tap density measurement. Tap density is a standard measure of the envelope mass density. The envelope mass density of an isotropic particle is defined as the mass of the particle divided by the minimum sphere envelope volume in which it can be enclosed. Features contributing to low tap density include irregular surface texture and porous structure.

Dry powder formulations ("DPFs") with large particle size have improved flowability characteristics, such as less aggregation (Visser, J., *Powder Technology* 58: 1-10 (1989)), easier aerosolization, and potentially less phagocytosis. Rudt, S. and R. H. Muller, *J. Controlled Release*, 22: 263-272 (1992); Tabata, Y., and Y. Ikada, *J. Biomed. Mater. Res.*, 22: 837-858 (1988). Dry powder aerosols for inhalation therapy are generally produced with mean diameters primarily in the range of less than 5 microns, although a preferred range is between one and ten microns in aerodynamic diameter. Ganderton, D., *J. Biopharmaceutical Sciences*, 3:101-105 (1992); Gonda, I. "Physico-Chemical Principles in Aerosol Delivery," in Topics in Pharmaceutical Sciences 1991, Crommelin, D. J. and K. K. Midha, Eds., Medpharm Scientific Publishers, Stuttgart, pp. 95-115 (1992). Large "carrier" particles (containing no drug) have been co-delivered with therapeutic aerosols to aid in achieving efficient aerosolization among other possible benefits. French, D. L., Edwards, D. A. and Niven, R. W., *J. Aerosol Sci.*, 27: 769-783 (1996). Particles with degradation and release times ranging from seconds to months can be designed and fabricated by established methods in the art.

Particles can consist of the osmotic agent, alone, or in combination with drug, surfactant, polymer, or combinations thereof. Representative surfactants include L-alpha.-phosphatidylcholine dipalmitoyl ("DPPC"),

diphosphatidyl glycerol (DPPG), 1,2-Dipalmitoyl-sn-glycero-3-phospho-L-serine (DPPS), 1,2-Dipalmitoyl-sn-glycero-3-phosphocholine (DSPC), 1,2-Distearoyl-sn-glycero-3-phosphoethanolamine (DSPE), 1-palmitoyl-2-oleoylphosphatidylcholine (POPC), fatty alcohols, polyoxyethylene-9-lauryl ether, surface active fatty acids, sorbitan trioleate (Span 85), glycocholate, surfactin, poloxomers, sorbitan fatty acid esters, tyloxapol, phospholipids, and alkylated sugars. Polymers may be tailored to optimize particle characteristics including: i) interactions between the agent to be delivered and the polymer to provide stabilization of the agent and retention of activity upon delivery; ii) rate of polymer degradation and thus drug release profile; iii) surface characteristics and targeting capabilities via chemical modification; and iv) particle porosity. Polymeric particles may be prepared using single and double emulsion solvent evaporation, spray drying, solvent extraction, solvent evaporation, phase separation, simple and complex coacervation, interfacial polymerization, and other methods well known to those of ordinary skill in the art. Particles may be made using methods for making microspheres or microcapsules known in the art. The preferred methods of manufacture are by spray drying and freeze drying, which entails using a solution containing the surfactant, spraying the solution onto a substrate to form droplets of the desired size, and removing the solvent.

### **III. Administration of Formulations to the Respiratory Tract**

#### **A. Methods of Administration**

The respiratory tract is the structure involved in the exchange of gases between the atmosphere and the blood stream. The lungs are branching structures ultimately ending with the alveoli where the exchange of gases occurs. The alveolar surface area is the largest in the respiratory system and is where drug absorption occurs. The alveoli are covered by a thin epithelium without cilia or a mucus blanket and secrete surfactant phospholipids. J.S. Patton & R.M. Platz. 1992. *Adv. Drug Del. Rev.* 8:179-196

The respiratory tract encompasses the upper airways, including the oropharynx and larynx, followed by the lower airways, which include the

trachea followed by bifurcations into the bronchi and bronchioli. The upper and lower airways are called the conducting airways. The terminal bronchioli then divide into respiratory bronchioli which lead to the ultimate respiratory zone, the alveoli or deep lung. The deep lung, or alveoli, is the primary target of inhaled therapeutic aerosols for systemic drug delivery.

The formulations are typically administered to an individual to deliver an effective amount to alter physical properties such as surface tension and viscosity of endogenous fluid in the upper airways, thereby enhancing delivery to the lungs and/or suppressing coughing and/or improving clearance from the lungs. Effectiveness can be measured using a system as described below. For example, saline can be administered in a volume of 1 gram to a normal adult. Exhalation of particles is then measured. Delivery is then optimized to minimize dose and particle number.

Formulations can be administered using a metered dose inhaler ("MDI"), a nebulizer, an aerosolizer, or using a dry powder inhaler. Suitable devices are commercially available and described in the literature.

Aerosol dosage, formulations and delivery systems may be selected for a particular therapeutic application, as described, for example, in Gonda, I. "Aerosols for delivery of therapeutic and diagnostic agents to the respiratory tract," in Critical Reviews in Therapeutic Drug Carrier Systems, 6:273-313, 1990; and in Moren, "Aerosol dosage forms and formulations," in: Aerosols in Medicine, Principles, Diagnosis and Therapy, Moren, et al., Eds. Esvier, Amsterdam, 1985.

Delivery is achieved by one of several methods, for example, using a metered dose inhaler including HFA propellant, a metered dose inhaler with non-HFA propellant, a nebulizer, a pressurized can, or a continuous sprayer. For example, the patient can mix a dried powder of pre-suspended therapeutic with solvent and then nebulize it. It may be more appropriate to use a pre-nebulized solution, regulating the dosage administered and avoiding possible loss of suspension. After nebulization, it may be possible to pressurize the aerosol and have it administered through a metered dose inhaler (MDI). Nebulizers create a fine mist from a solution or suspension,



which is inhaled by the patient. The devices described in U.S. Patent No. 5,709,202 to Lloyd, et al., can be used. An MDI typically includes a pressurized canister having a meter valve, wherein the canister is filled with the solution or suspension and a propellant. The solvent itself may function  
5 as the propellant, or the composition may be combined with a propellant, such as FREON® (E. I. Du Pont De Nemours and Co. Corp.). The composition is a fine mist when released from the canister due to the release in pressure. The propellant and solvent may wholly or partially evaporate due to the decrease in pressure.

10 In an alternative embodiment, the formulation is in the form of salt or osmotically active material particles which are dispersed on or in an inert substrate, which is placed over the nose and/or mouth and the formulation particles inhaled. The inert substrate is preferably a biodegradable or disposable woven or non-woven fabric and more preferably the fabric is  
15 formed of a cellulosic-type material. An example is tissues currently sold which contain lotion to minimize irritation following frequent use. These formulations can be packaged and sold individually or in packages similar to tissue or baby wipe packages, which are easily adapted for use with a liquid solution or suspension.

20 Individuals to be treated include those at risk of infection, those with a viral or bacterial infection, allergy patients, asthma patients, and individuals working with immunocompromised patients or infected patients.

The formulation may be administered to humans or animals such as racehorses, breeding livestock, or endangered captive animals to protect  
25 these animals from infection by viral shedding. This may be accomplished by placing a nebulizer system near watering stations and triggering production of the aerosol as animals either approach or leave the station. Formulation may be sprayed over the animals as they walk through chutes or pens, or sprayed from spray trucks or even crop dusting type airplanes.  
30 Individual battery powered sprayers that are currently used to spray insecticides may be adapted for use in administering the solutions to the animals to minimize bioaerosol formation and/or dispersion.

The formulation may be administered to humans or animals at the onset of viral or bacterial outbreak to prevent spread of the disease to epidemic levels. Animals within a 10-kilometer radius of a FMD outbreak are currently deemed infected. These animals are subsequently slaughtered and disinfected. This aerosol system may be administered immediately to animals within this 10-kilometer radius zone and a further prescribed buffer zone outside this area to assure containment of the outbreak. The aerosol can then be administered for as long as is necessary to ensure success, i.e. beyond the normal period between first infection and symptom expression.

The formulation may be administered to humans or animals by creating an aqueous environment in which the humans and animals move or remain for sufficient periods of time to sufficiently hydrate the lungs. This atmosphere might be created by use of a nebulizer or even a humidifier.

Although described primarily with reference to pulmonary administration, it is understood that the formulations may be administered to individual animals or humans through inhalation; parenteral, oral, rectal, vaginal or topical administration; or by administration to the ocular space.

#### **IV. Methods and Devices for Screening for “Over Producers”**

##### **A. Methods**

Diagnosis of animals or humans who have an enhanced propensity to exhale aerosols (referred to herein as “over producers”, “super-producers”, or “superspreaders”) can be done by screening for a number of factors including the measurement of expired air and inspired air, the assessment of exhaled particle numbers, the assessment of exhaled particle size, the assessment of tidal volume and respiratory frequency during sampling, and the assessment of viral and bacterial infectivity. The assessment of exhaled particle numbers is done at a respiratory flow rate of about 10 to about 120 liters per minutes (LPM).

##### **B. Devices**

A device with sufficient sensitivity to accurately count sub-micron sized particles was designed and assembled as described in the examples. Preferably the device is portable and operates on batteries. The measurement

of particle number and particle size can be done by infrared spectroscopy, laser diffraction, or light scattering

*In vitro* testing of bioaerosol transmission

The following *in vitro* method can be used to test the effectiveness of delivering saline or other solutions of an osmotically active material on bioaerosol generation in the airways. A “cough machine” (M. King, J.M. Zahm, D. Pierrot, S. Vaquez-Girod, E. Puchelle. *Biorheology*. (1989) 26:737-745) is used to control air speed experienced by simulated mucus lining of the airway. Labeled nanoparticles can be incorporated into the fluid, and a filter placed at the exit of the cough machine to collect the aerosol droplets generated. A variety of compounds can be added to alter shear viscosity, elongational viscosity, and surface tension. The test is repeated at varying air velocities, below, including, and above 25 m/s.

Toxicity studies

Compounds to be administered can be tested for non-toxicity. For example, preliminary *in vitro* studies can be conducted to test the toxicity of solutions upon addition to monolayers of fibroblast cells. NIH 3T3 fibroblasts are plated onto glass Lab-Tek™ coverslip chambers (NUNC, Rochester, NY) and grown to confluence. The cells are then exposed to a solution in 10% FBS DMEM for 10 seconds and returned to the incubator after several washes with 10% FBS in DMEM. After 15 minutes the cells are exposed to 10  $\mu$ M Cell-Tracker™ Green CMFDA (Molecular Probes, Eugene, OR) for 30 min. The cells are then washed several times with 10% FBS DMEM and placed in a 37°C, 5% CO<sub>2</sub> microscope chamber. The CMFDA stain readily enters the cell and if the cell is alive, the stain becomes enzymatically modified and cannot leave. Thus viable cells will fluoresce brightly while dead cells will not. The cells are imaged with an inverted fluorescence microscope.

*In vivo* toxicity studies determine which of the most effective formulations of the *in vitro* studies are the least toxic. Animals will be administered the prepared formulations and intravenous blood samples will

be collected. Also, tracheal lavage will provide information about damage to lung tissue resulting from administration of the preparations.

Treatment is continued for as long as there is risk of infection or spread of disease, with treatment repeated as necessary to prevent or limit viral shedding. In the case of asthma, allergy and other pulmonary disorders, treatment will be continued to maintain the desired pulmonary parameters.

The present invention will be further understood by reference to the following non-limiting examples.

### Examples

#### 10 **Example 1: *In Vitro* Simulation**

As shown in Figure 1, a simulated cough machine system was designed similar to that described by King Am. J. Respir. Crit. Care Med. 156(1):173-7 (1997). An air-tight 6.25-liter Plexiglas tank equipped with a digital pressure gauge and pressure relief valve was constructed to serve as the capacitance function of the lungs. To pressurize the tank, a grade dry compressed air cylinder with regulator was connected to the inlet. At the outlet of the tank, an Asco two-way normally-closed solenoid valve (8210G94) with a sufficient Cv flow factor was connected for gas release. The solenoid valve was wired using a typical 120V, 60Hz light switch. Connected to the outflow of the solenoid valve was a Fleisch no. 4 pneumotachograph, which created a Poiseuille flow needed to examine the "cough" profile. The outlet of the Fleisch tube was connected to a 1/4" NPT entrance to our model trachea. A Validyne DP45-14 differential pressure transducer measured the pressure drop through the Fleisch tube. A Validyne CD15 sine wave carrier demodulator was used to amplify this signal to the data acquisition software. Weak polymeric gels with rheological properties similar to tracheobronchial mucus were prepared as described by King et al Nurs Res. 31(6):324-9 (1982). Locust bean gum (LBG) (Fluka BioChemika) solutions were crosslinked with sodium tetraborate ( $\text{Na}_2\text{B}_4\text{O}_7$ ) (J.T.Baker). LBG at 2% wt/vol was dissolved in boiling Milli-Q distilled water. A concentrated sodium tetraborate solution was prepared in Milli-Q distilled water. After the LBG solution cooled to room temperature, small amounts of

sodium tetraborate solution were added and the mixture was slowly rotated for 1 minute. The still watery mucus simulant was then pipetted onto the model trachea creating simulant depth based on simple trough geometry. Mucus simulant layers were allowed 30 minutes to crosslink prior to

5 initiation of "cough" experiments. At this point,  $t=0$  min, time points were measured, followed by  $t=30$  min and  $t=60$  min. Final concentrations of sodium tetraborate ranged from 1-3 mM. An acrylic model trachea was designed 30 cm long with interior width and height of 1.6 cm. The model trachea formed a rectangular shaped tube with a separate top to fit, allowing

10 for easy access to the mucus simulant layer. A gasket and C-clamps were used to create an air-tight seal. A rectangular cross-section was chosen to enable uniform mucus simulant height and to avoid problems associated with round tubes and gravity drainage. The cross-sectional area of the model trachea was also physiologically relevant. The end of the model trachea

15 remained open to the atmosphere. Nebulized solutions were delivered to the mucus simulant via a PARI LC Jet nebulizer and Proneb Ultra compressor. Formulations included normal isotonic 0.9% saline (VWR) and 100 mg/mL of synthetic phospholipids 1,2-Dipalmitoyl-sn-glycero-3-phosphocholine/1-Palmitoyl-2-oleoyl-sn-glycero-3-phosphoglycerol (DPPC/POPG) (Genzyme)

20 7/3 wt% suspended in isotonic saline. 3 mL of the chosen formulation was pipetted into the nebulizer and aerosolized until nebulizer sputter through the open-ended but clamped model trachea trough on the layer of mucus simulant. The model trachea was then attached to the outlet of the Fleisch tube prior to  $t=0$  min experiments. As well,  $t=30$  min and  $t=60$  min (post-

25 dose) experiments were performed.

A Sympatec HELOS/KF laser diffraction particle sizer was used to size the created mucus simulant bioaerosols. The Fraunhofer method for sizing diffracted particles was used. The HELOS was equipped with an R2 submicron window module enabling a measuring range of 0.25-87.5  $\mu\text{m}$ .

30 Prior to "cough" experiments, the end of the model trachea was adjusted to be no more than 3 cms from the laser beam. As well, the bottom of the model trachea was aligned with the 2.2 mm laser beam using support jacks

and levels. Dispersed bioaerosols were collected after passing through the diffraction beam using a vacuum connected to an inertial cyclone followed by a HEPA filter. Before each run, the laser was referenced for 5 s to ambient conditions. Measurement began after a specified trigger condition of optical concentration ( $C_{opt} \geq 0.2\%$ ) and stopped 2 s after  $C_{opt} \leq 0.2\%$ . Sympatec WINDOX software was used to create cumulative and density distribution graphs versus log particle size by volume.

A typical cough profile, consisting of a biphasic burst of air, was passed over the 1.5 mm layer of mucus simulant. The initial flow of air possessed a flow rate of about 12 L/s for 30-50 ms. The second phase lasted 200-500 ms and then rapidly decayed. A representative actual cough profile is compared with a simulated cough profile (5psi tank pressure) in Figure 2.

Bioaerosol particle concentration following three coughs was measured over time (Figure 3) in the case of an undisturbed mucus simulant, and in the cases of saline delivery (Figure 3) and surfactant delivery (not shown). In the undisturbed case, bioaerosol particle size remains constant over time with a median size of about 400 nanometers. Following the addition of saline, bioaerosol particle size increases from 1 micron ( $t=0$ ) to about 60 microns ( $t=30$  min) and then diminishes to 30 microns ( $t=60$  min).

These *in vitro* results show that saline delivered to a mucus layer causes a substantial increase in particle size on breakup, possibly owing to an increase in surface tension. As indicated by the *in vivo* results, the larger size droplets are less capable of exiting the mouth. Therefore, delivery of the solution serves to significantly lower the number of expired particles.

## **Example 2: Reduction of Exhaled Aerosol Particles in Human Study**

A proof of concept study of exhaled aerosol particle production was performed using 12 healthy subjects. The objectives of the study were (1) to determine the nature of exhaled bioaerosol particles (size distribution and number); (2) to validate the utility of a device that is sensitive enough to accurately count the exhaled particles; (3) to assess the baseline count of particles exhaled from the healthy lung; and (4) to measure the effect of two exogenously administered treatment aerosols on exhaled particle count

suppression. Experiments were performed with different particle detectors to determine average particles per liter and average particle size for healthy human subjects. Following the inspiration of particle-free air, healthy subjects breathe out as little as 1-5 particles per liter, with an average size of 200-400 nm in diameter. Significant variations occur in numbers of particles from subject to subject, so that some subjects exhale as many as 30,000 particles per liter, again predominantly of submicron particle size. A device with sufficient sensitivity to accurately count sub-micron sized particles was designed and assembled. The LASER component of the device was calibrated in accordance with manufacturer procedures (Climet Instruments Company, Redlands, CA). This device accurately measured particles in the range of 150-500 nm with a sensitivity of 1 particle/liter. A series of filters eliminated all background particle noise.

Following protocol IRB approval, 12 healthy subjects were enrolled in the study. Inclusion criteria were good health, age 18 – 65 years, normal lung function ( $FEV_1$  predicted > 80%), informed consent and capability to perform the measurements. Exclusion criteria were presence or a history of significant pulmonary disease (e.g. asthma, COPD, cystic fibrosis), cardiovascular disease, acute or chronic infection of the respiratory tract, and pregnant or lactating females. One individual was not able to complete the entire dosing regimen and therefore was excluded from the data analysis.

Following a complete physical exam, the subjects were randomized into two groups: those to initially receive prototype formulation 1 and those to receive prototype formulation 2. Baseline exhaled particle production was measured after a two minute “wash out” period on the device. The assessment was made over a two minute period with the per-minute count derived from the average of the two minutes. Following the baseline measurement, the prototype formulation was administered over a six minute period using a commercial aqueous nebulizer (Pari Respiratory Equipment, Starnberg, Germany). Formulation 1 consisted of an isotonic saline solution. Formulation 2 consisted of a combination of phospholipids suspended in an isotonic saline vehicle. Following administration, exhaled particle counts

were assessed 5 minutes, 30 minutes, one hour, two hours, and three hours after the single administration.

As shown in Figure 4A, substantial inter-subject variability was found in baseline particle counts. The data shown are measurements made prior to administration of one of the test aerosols. This baseline expired particle result points to the existence of “super producers” of exhaled aerosols. In this study “super-producers” were defined as subjects exhaling more than 1,000 particles/liter at baseline measurement. Figure 4B shows the individual particle counts for subjects receiving Formulation 1. The data indicate that a simple formulation of exogenously applied aerosol can suppress exhaled particle counts.

Figure 5A shows the effect of prototype formulation 1 on the two “super-producers” found at baseline in this group. These data indicate that the prototype formulation may exert a more pronounced effect on super-producers.

Similar results were found on delivery of formulation 2. Figure 5B summarizes the percent change (versus baseline) of the cumulative exhaled particle counts for the “super-producers” identified in the two treatment groups.

Results from this study demonstrate that exhaled particles can be accurately measured using a laser-detection system, that these particles are predominantly less than 1 micron in diameter, and that the number of these particles varies substantially from subject to subject. “Super-producing” subjects respond most markedly to delivery of an aerosol that modifies the physical properties of the surface of the lining fluid of the lungs. Such super-producers might bear significant responsibility for pathogen shedding and transmission in a population of infected patients. These data also demonstrate that suppressing aerosol exhalation is practical with relatively simple and safe exogenously administered aerosol formulations.

### **Example 3: Large Animal Study**

Seven (7) Holstein bull calves were anesthetized, intubated, and screened for baseline particle exhalation by optical laser counting. Animals



were subsequently untreated (sham) or treated with a nebulized aerosol of saline at one of three doses (1.8 minutes, 6.0 minutes or 12.0 minutes).

During the sham dosage, the animals were handled in the same manner as they were when the dosages of the isotonic saline solution were

- 5 administered. One animal was dosed per day and nebulizer doses were randomized throughout the exposure period (see Table 1 for dosing schedule). Each animal was slated to receive all doses during the duration of the study. Following the administration of each dose, exhaled particle counts were monitored at discrete timepoints (0, 15, 30, 45, 60, 90, 120) through  
10 180 minutes.

The exposure matrix for the animals included in the study is found in Table 1. The dosing occurred over a 57 day period, with at least a 7 day interval between dosages. Each animal (n=7) received each dose at least once during the duration of dosing, with the exception of the omission of one  
15 6.0 minute dose (see animal no. 1736) and one 12.0 minute dose (see animal no. 1735). These two were excluded due to unexpected problems with the ventilator and/or anesthesia equipment.

**Table 1: Dosing Regime for Large Animals**

Animal No.	Dosage			
	Sham	1.8 min.	6.0 min.	12.0 min.
1731	Day 17	Day 3	Day 10	Day 25
1732	Day 7	Day 21	Day 1	Day 14
1735	Day 18	Day 11	Day 4	N/A
1736	Day 23	Day 2	N/A	Day 9
1738	Day 8	Day 15	Day 36	Day 25
1739	Day 20	Day 38	Day 30	Day 45
1741	Day 50	Day 35	Day 57	Day 42

## 20 **Results**

Figure 6A show the particle count over time for each animal after it received a sham dosage. Each timepoint typically represents the mean of at least three particle count determinations. The data in Figure 6A shows that

certain individual animals inherently produce more particles than others (“superspreaders”). Additionally, the data show that throughout the assessment period, quiescently breathing anesthetized animals maintain a relatively stable exhaled particle output (see e.g. Animal nos. 1731, 1735, 1738, 1739, and 1741).

Figure 6B represents the mean percent change in exhaled particle counts over time following each treatment. Each data point represents the mean of six to seven measurements from the treatment group. All animals had returned to baseline by 180 minutes post treatment. The data suggest that the 6.0 minute treatment period provides an adequate dose to prevent the exhalation of particles for at least 150 minutes post-treatment. The other treatments appear to be either too short or too long to provide an effective, lasting suppression of aerosol exhalation.

### ***Conclusion***

The study conducted in cattle demonstrates the efficacy of isotonic saline on the formation of exhaled aerosols in spontaneously breathing animals relevant to livestock herds. Based on the results, delivery of isotonic saline can markedly diminish the number of expired aerosol particles in a dose-responsive manner. In addition, this large animal dosing system allows for repeated controlled exposures. By using each animal as its own control via the daily pre-exposure baseline and the sham exposure, the inherent variability associated with particle exhalation can be understood. The data suggests that 6.0 minutes of saline nebulization diminishes particle exhalation for a minimum of 120 minutes in cows.

We claim:

1. A biocompatible non-surfactant formulation that when administered to a human or other animal, dilutes endogenous surfactant fluid, to alter surface tension, surface elasticity, or bulk viscosity, thereby decreasing aerosol exhalation.
2. The formulation of claim 1 selected from the group consisting of aqueous solutions, dry powders, vapors, aqueous suspensions, non-toxic organic solutions or suspensions, and solid dosage form other than dry powder.
3. The formulation of claim 1 formulated for administration to a region selected from the group consisting of the respiratory tract, the gastrointestinal tract, and the oropharynx or nasal cavities.
4. The formulation of claim 1 comprising an effective amount of a compound selected from the group consisting of salts and sugars to decrease aerosol exhalation.
5. The formulation of claim 1 further comprising an agent selected from the group consisting of surfactants and phospholipids.
6. The formulation of claim 1 comprising an active agent selected from the group consisting of nucleic acids, proteins, carbohydrates, synthetic polymers, amino acids, inorganic substances, and organic substances.
7. The formulation of claim 6 wherein the concentration of the active agent ranges from about 0.01% to about 20% by weight.
8. The formulation of claim 7 wherein the concentration of active agent ranges from between 0.9% to about 10%.
9. The formulation of claim 1 in a form selected from the group consisting of particles dispersed or in an inert substrate, droplets dispersed on or in an inert substrate, vapor dispersed on or in an inert substrate, and mist dispersed on or in an inert substrate.
10. The formulation of claim 6 wherein the active agent is selected from the group consisting of antivirals, antibiotics, bronchodilators,

antihistamines, cough suppressants, anti-inflammatories, expectorants, and vaccines..

11. The formulation of claim 1 in an effective amount to limit infectivity of an infectious agent.
12. The formulation of claim 1 wherein the formulation is saline.
13. The formulation of claim 1 wherein the formulation comprises an aqueous solution delivered as an aerosol with particles having a diameter between about 0.1 and about 30 microns, most preferably between about 1 and about 10 microns.
14. The formulation of claim 1 wherein the formulation is delivered in an effective duration to suppress exhaled bioaerosol formation between 0 and 20 minutes, most preferably between 0-3 minutes.
15. The formulation of claim 1 in a device selected from the group consisting of a metered dose inhaler including HFA propellant, a metered dose inhaler with non-HFA propellant, a nebulizer, a pressurized can, and a continuous sprayer.
16. The formulation of claim 1 wherein the formulation consists of a dry powder of mass median aerodynamic diameter of less than about 10 microns.
17. The formulation of claim 1 comprising a powder selected from the group consisting of isotonic dry powder, a hypertonic dry powder, a hyptonic dry powder, a dry powder including osmotically active excipient, a dry powder of an excipient that changes surface tension, a dry powder of an excipient that changes viscosity, a dry powder of an excipient that changes surface pressure, or a dry powder of an excipient that changes surface energy.
18. The formulation of claim 1 wherein the formulation is in a device selected from the group consisting of a single-dose dry powder inhaler and multi-dose dry powder inhaler.
19. The formulation of claim 1 wherein the formulation is in a vaporizer or a vapor inhaler or a device selected from the group consisting of a metered dose inhaler including HFA propellant, a metered dose inhaler

with non-HFA propellant, a nebulizer, a pressurized can, and a continuous sprayer and is selected from the group consisting of a vapor including osmotically active excipient, a vapor that changes surface tension, a vapor that changes viscosity, a vapor that changes surface pressure, and a vapor that changes surface energy.

20. The formulation of claim 1 comprising a suspension selected from the group comprising an isotonic suspension, a hypertonic suspension, a hypotonic suspension, an aqueous suspension including osmotically active excipient, an aqueous suspension of an excipient that changes surface tension, an aqueous suspension of an excipient that changes surface pressure and aqueous suspension of an excipient that changes surface energy, wherein the formulation is delivered as an aerosol with particles having a diameter between approximately 0.1 and 30 microns, most preferable between approximately 1 and 10 microns in a device selected from the group consisting of metered dose inhaler including HFA propellant, a metered dose inhaler with non-HFA propellant, a nebulizer, a pressurized can, and a continuous sprayer.

21. The formulation of claim 1 comprising a solution or suspension selected from the group consisting of a non-toxic organic solution or suspension including an osmotically active excipient, a non-toxic organic solution or suspension of an excipient that changes surface tension, a non-toxic organic solution or suspension of an excipient that changes viscosity, a non-toxic organic solution or suspension of an excipient that changes surface pressure, a non-toxic organic solution or suspension of an excipient that changes surface energy, and non-toxic organic solution or suspensionm delivered as an aerosol in a device selected from the group consisting of metered dose inhaler including HFA propellant, a metered dose inhaler with non-HFA propellant, a nebulizer, a pressurized can, and a continuous sprayer with particles having a diameter most preferably between approximately 1 and 10 microns.

22. An inert substrate comprising an effective amount of a particulate composition for administration to the nose or mouth to dilute endogenous surfactant fluid, to alter surface tension, surface elasticity, or bulk viscosity, thereby decreasing aerosol exhalation.

23. The substrate of claim 22 wherein the composition comprises a material selected from the group consisting of salts, sugars and other osmotically active materials.

24. The substrate of claim 23 wherein the concentration of composition on or in the substrate ranges from about 0.01% to about 20% by weight, preferably between 0.9% to about 10%.

25. The substrate of claim 22 wherein the substrate comprises a biodegradable or disposable woven or non-woven fabric.

26. The substrate of claim 25 wherein the fabric is formed of a cellulose type material

27. The substrate of claim 22 further comprising at least one bioactive compound.

28. The substrate of claim 27 wherein the bioactive agent is selected from the group consisting of an antiviral, an antibiotic, a bronchodilator, a steroid, and a vaccine.

29. The substrate of claim 22 further comprising a lotion or lubricant for application to the skin.

30. The substrate of claim 22 comprising particulate surfactant in an effective amount to limit infectivity of an infectious agent.

31. A method of decreasing exhalation of particles in an individual having a respiratory disease comprising administering to the individual an effective amount of a biocompatible non-surfactant formulation that dilutes endogenous surfactant fluid, to alter surface tension, surface elasticity, or bulk viscosity, thereby decreasing aerosol exhalation.

32. The method of claim 31 wherein the respiratory disease is an infection with an agent selected from the group consisting of the agents causing tuberculosis, SARS, influenza, cytomegalovirus, respiratory

syncytial virus, African swine fever, coronavirus, rhinovirus, tularemia, bubonic plague, anthrax, and foot and mouth disease.

33. The method of claim 13 wherein the respiratory disease is selected from the group consisting of allergy, asthma, cystic fibrosis, chronic bronchitis, emphysema, and acute respiratory distress syndrome.

34. The method of claim 31 wherein the formulation alters physical properties selected from the group consisting of the surface tension of respiratory tract lining fluid, the viscosity of the respiratory tract lining fluid, the surface elasticity of the respiratory tract lining fluid, the surface pressure of the respiratory tract lining fluid, the surface energy of the respiratory tract lining fluid, the osmolarity of the respiratory tract lining fluid, the osmotic activity of respiratory tract cell types, the production of airway lining fluid, transport of bioaerosols within an individual from sites of upper airway deposition to lung parenchyma..

35. The method of claim 31 where the formulation creates a coating on the respiratory tract lining fluid.

36. The method of claim 31 wherein the formulation is applied as a solution or suspension parenterally, orally, rectally, vaginally, topically, or by and inhalation.

37. The method of claim 36 wherein the solution or suspension is administered to the ocular space.

38. The method of claim 33 wherein the formulation is administered in a building, tent, or other facility.

39. A method for the diagnosis of animals or humans who have an enhanced propensity to exhale aerosols comprising screening for at least one characteristic selected from the group consisting of the measurement of expired air and inspired air, assessment of exhaled particle numbers, assessment of exhaled particle size, assessment of tidal volume and respiratory frequency during sampling.

40. The method of claim 39 comprising assessing exhaled particle numbers at a respiratory flow rate of about 10 to about 120 LPM.

41. The method of claim 39 comprising assessment of infectivity of exhaled aerosol.

42. The method of claim 39 comprising measuring bacterial or viral infectivity.

43. A device for the measurement of exhaled particle number and particle size according to the method of claim 39.



FIGURE 1

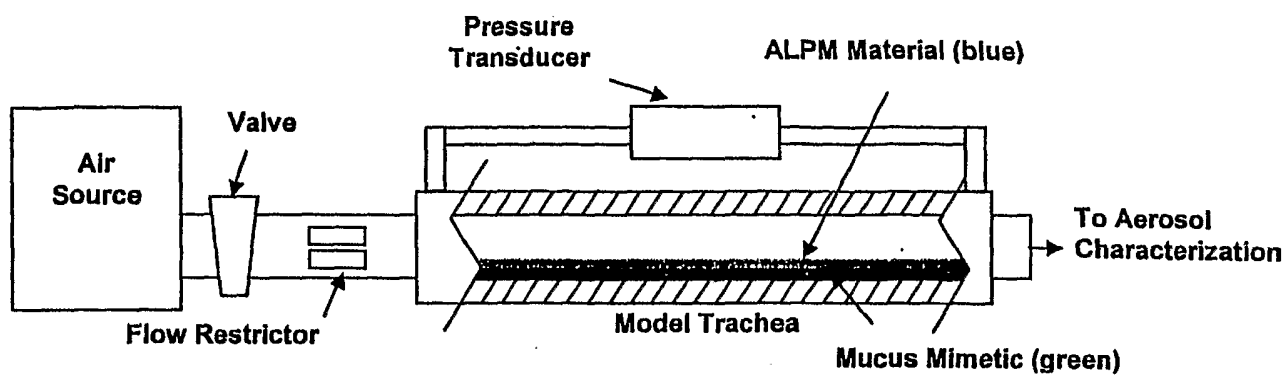


FIGURE 2

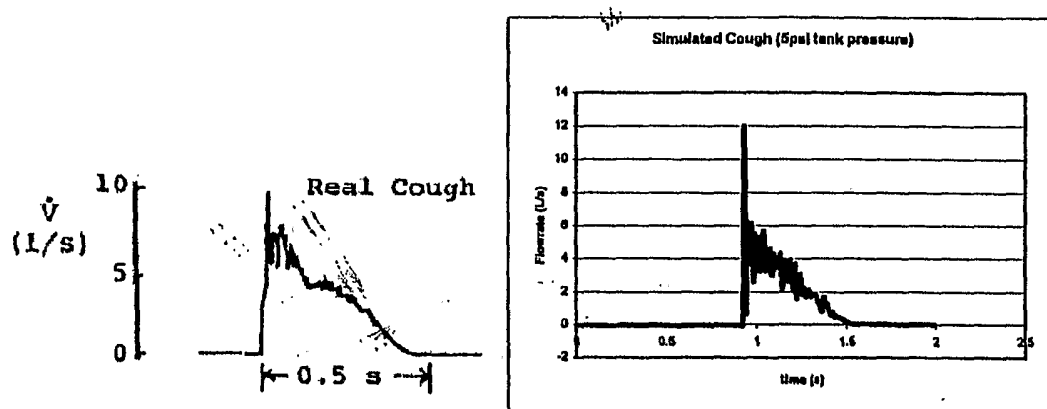


FIGURE 3

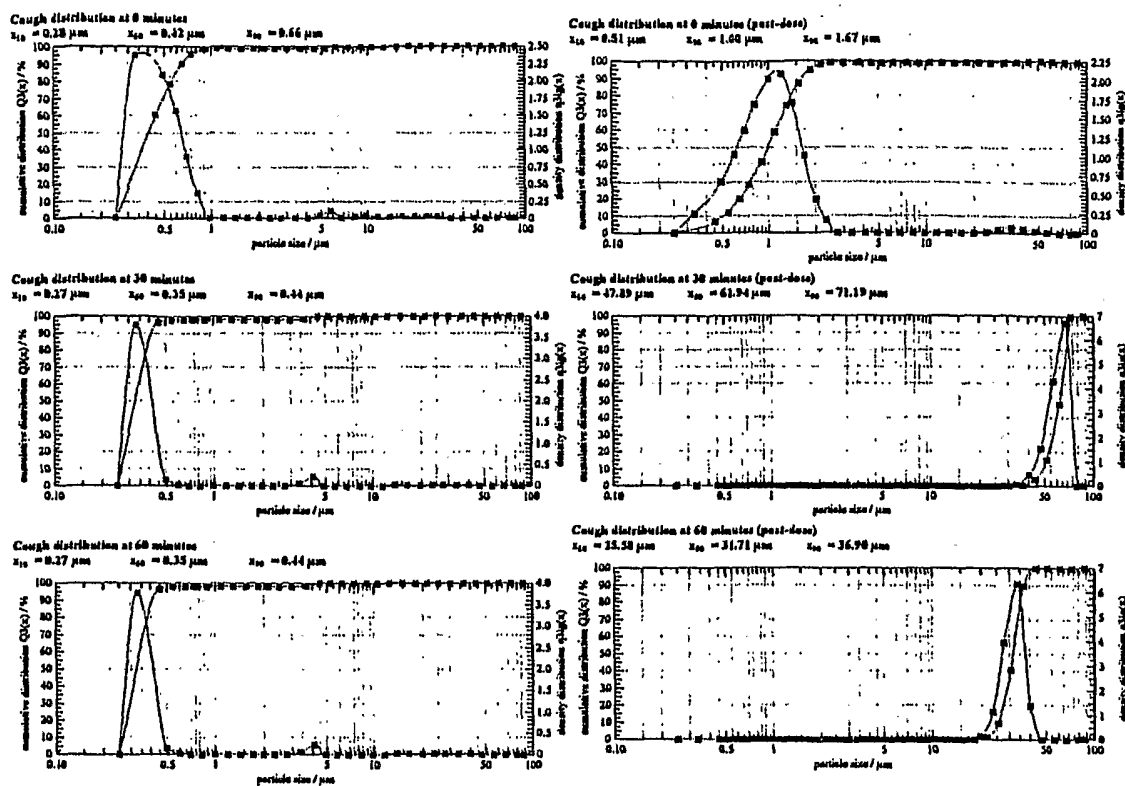


FIGURE 4

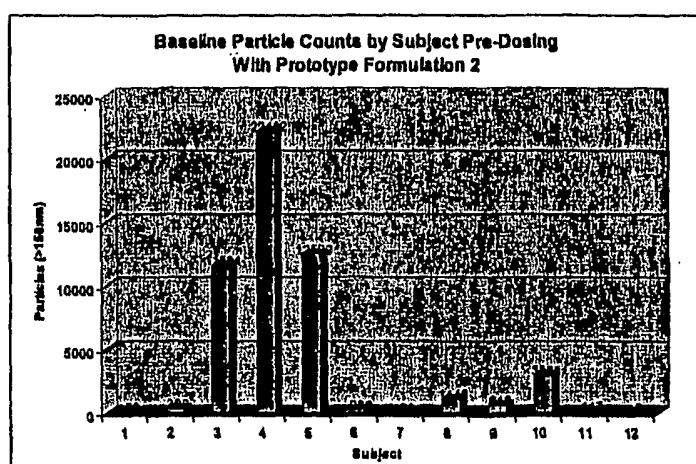


FIGURE 5

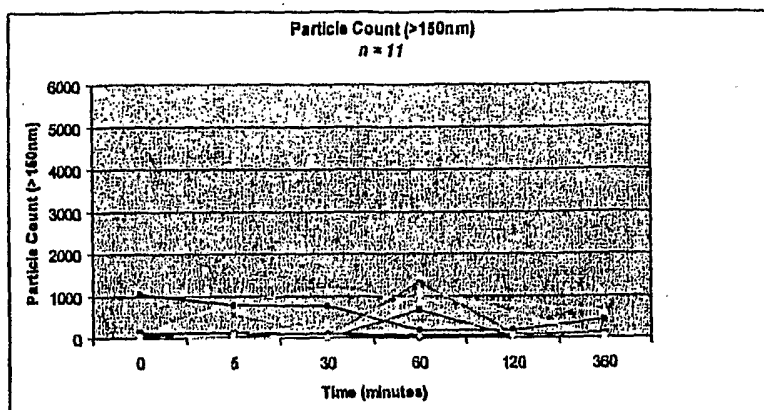


FIGURE 6

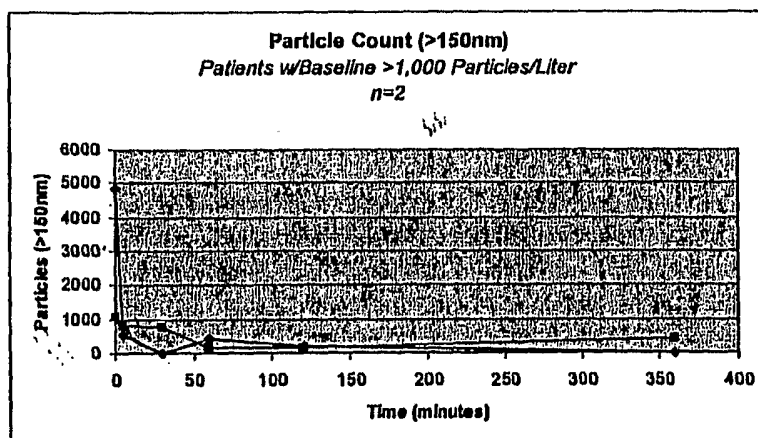
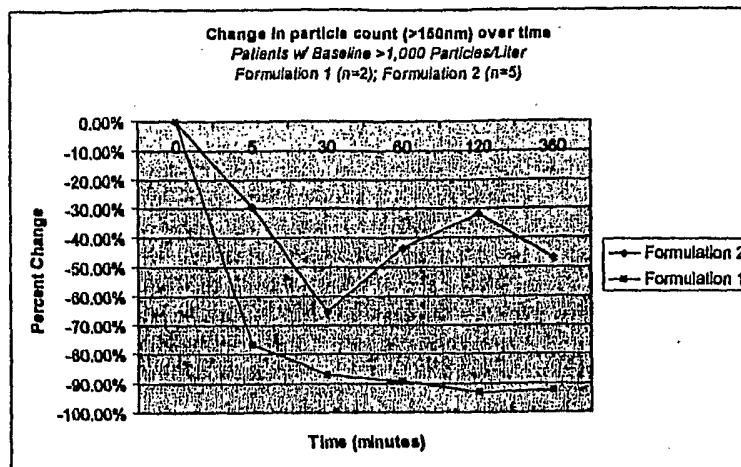


FIGURE 7



## Sham Exposure Particle Counts (N=7)

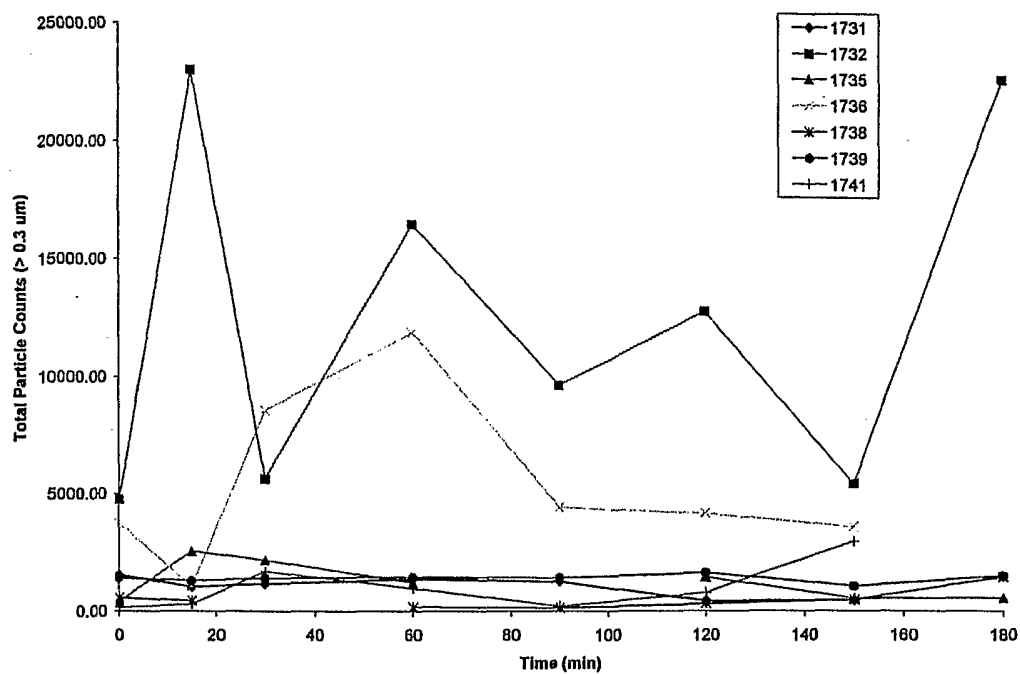


Fig. 8A

## % Baseline Dose Data (n=6-7)

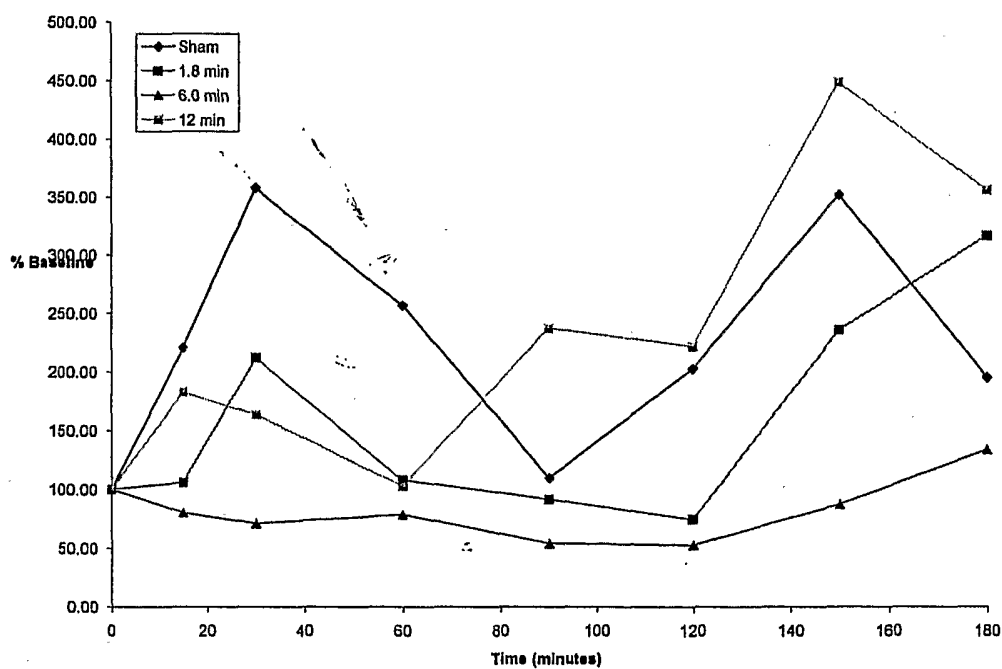


Fig. 8B