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(19) **United States**(12) **Patent Application Publication****Rava et al.**(10) **Pub. No.: US 2005/0282156 A1**(43) **Pub. Date: Dec. 22, 2005**(54) **METHODS FOR MAKING A DEVICE FOR
CONCURRENTLY PROCESSING MULTIPLE
BIOLOGICAL CHIP ASSAYS**(75) Inventors: **Richard P. Rava**, San Jose, CA (US);
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SANTA CLARA, CA 95051 (US)(73) Assignee: **Affymetrix, INC.**, Santa Clara, CA(21) Appl. No.: **11/173,366**(22) Filed: **Jul. 1, 2005****Related U.S. Application Data**(63) Continuation of application No. 11/044,834, filed on
Jan. 26, 2005, which is a continuation of application
No. 10/997,492, filed on Nov. 24, 2004, which is a
continuation of application No. 10/795,086, filed on

Mar. 5, 2004, which is a continuation of application
No. 10/157,252, filed on May 28, 2002, now Pat. No.
6,720,149, which is a continuation of application No.
09/247,430, filed on Feb. 10, 1999, now abandoned,
which is a continuation of application No. 08/630,
051, filed on Apr. 9, 1996, now Pat. No. 5,874,219,
which is a continuation of application No. 08/476,
850, filed on Jun. 7, 1995, now Pat. No. 5,545,531.

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C12M 1/34
(52) **U.S. Cl.** **435/5**; 435/6; 435/287.2(57) **ABSTRACT**

Methods for concurrently processing multiple biological
chip assays by providing a biological chip plate comprising
a plurality of test wells, each test well having a biological
chip having a molecular probe array; introducing samples
into the test wells, subjecting the biological chip plate to
manipulation by a fluid handling device that automatically
performs steps to carry out reactions between target mol-
ecules in the samples and probes; and subjecting the bio-
logical chip plate to a biological chip plate reader that
interrogates the probe arrays to detect any reactions between
target molecules and probes.

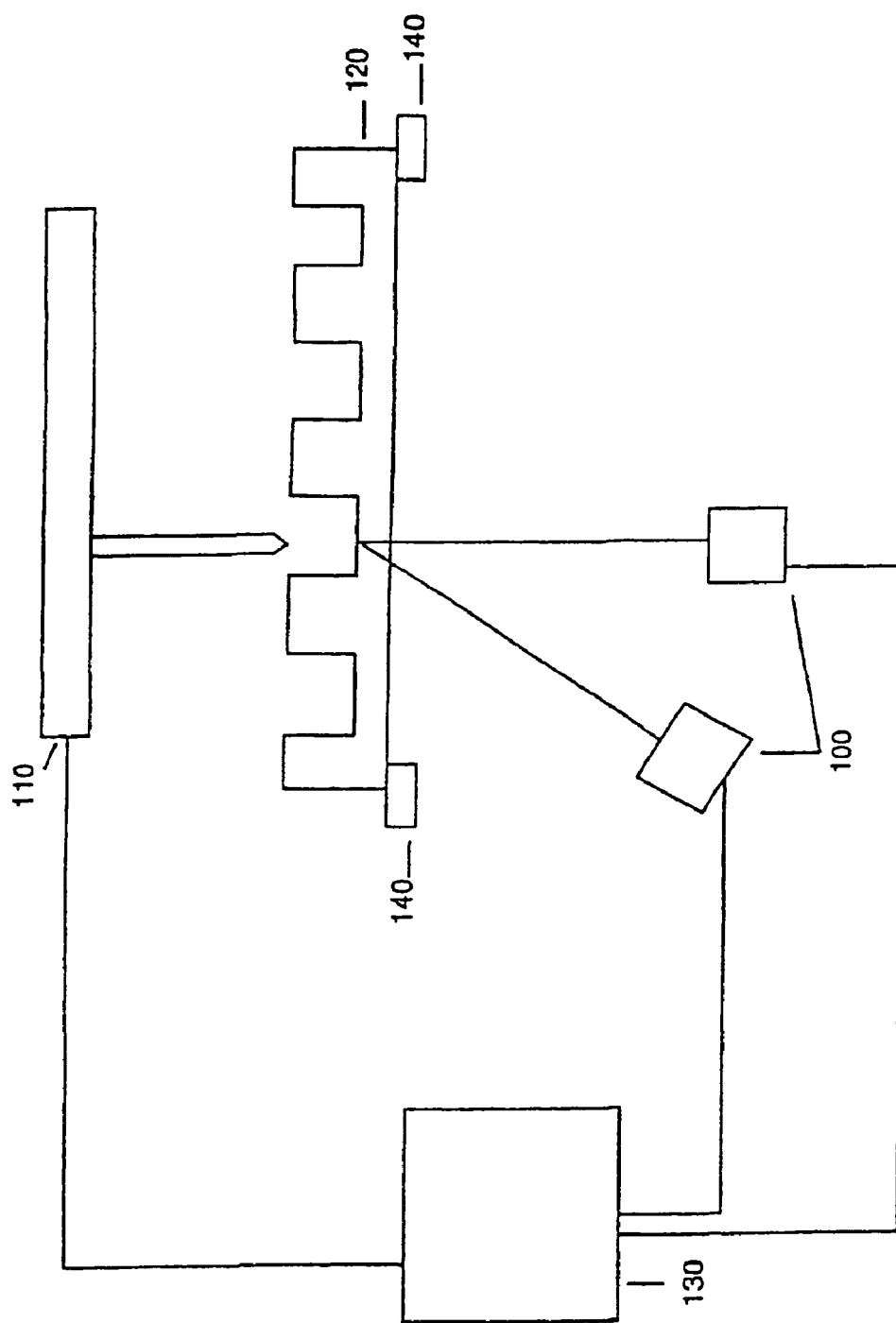


Figure 1

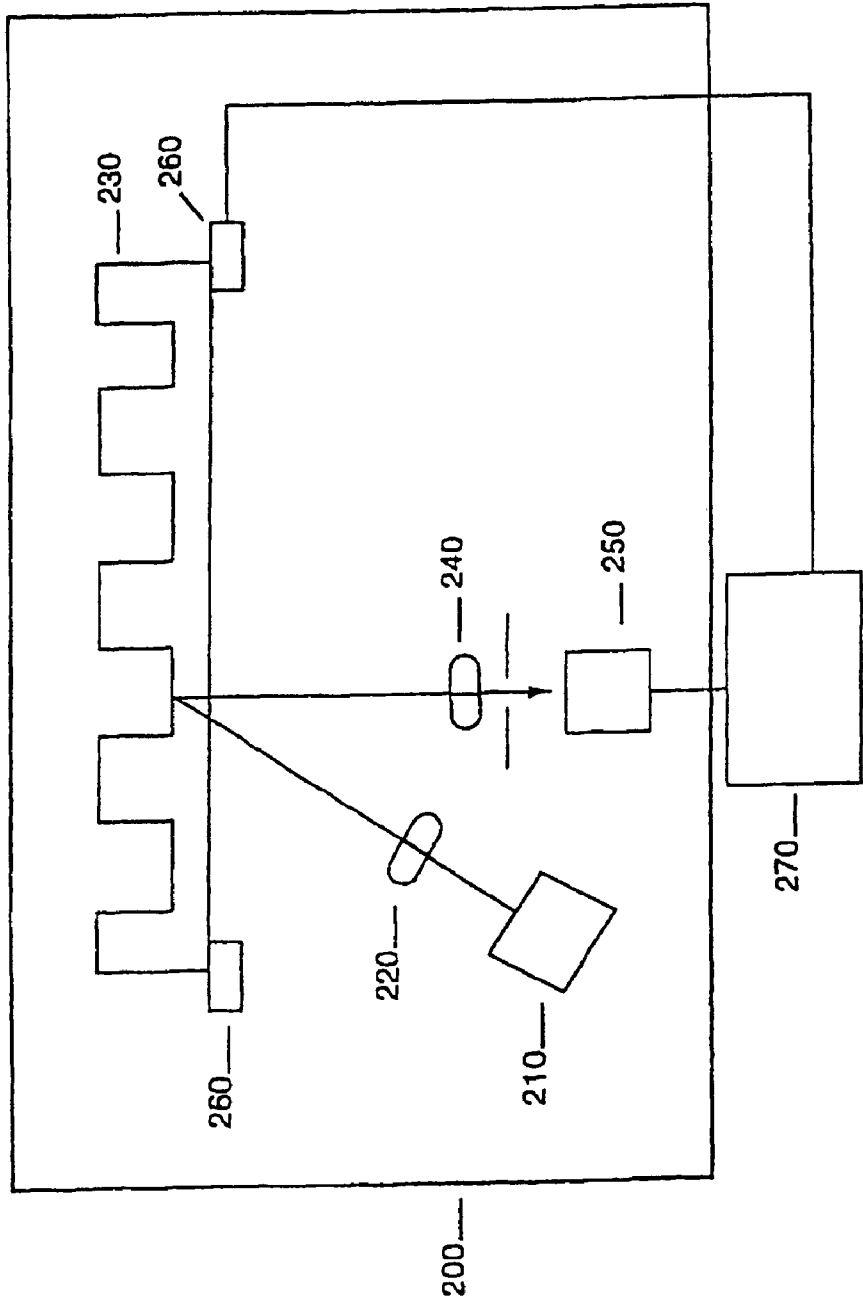


Figure 2

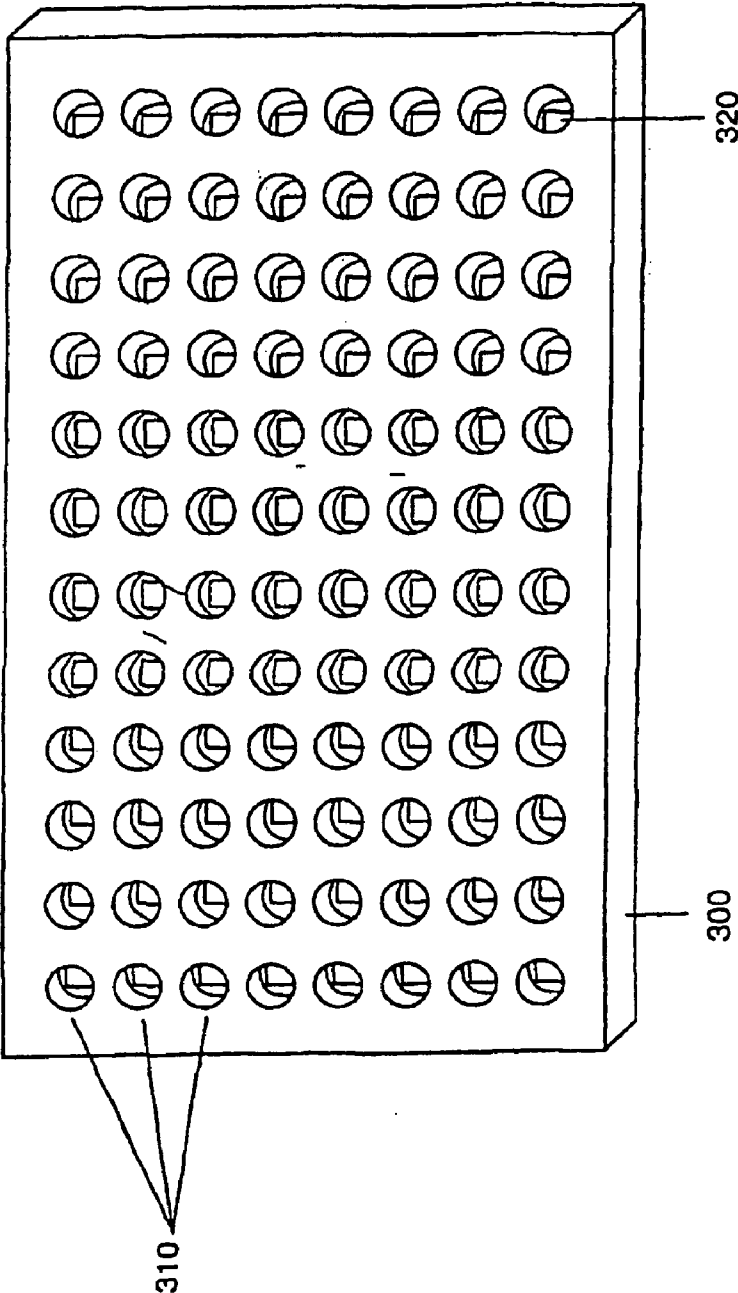


Figure 3

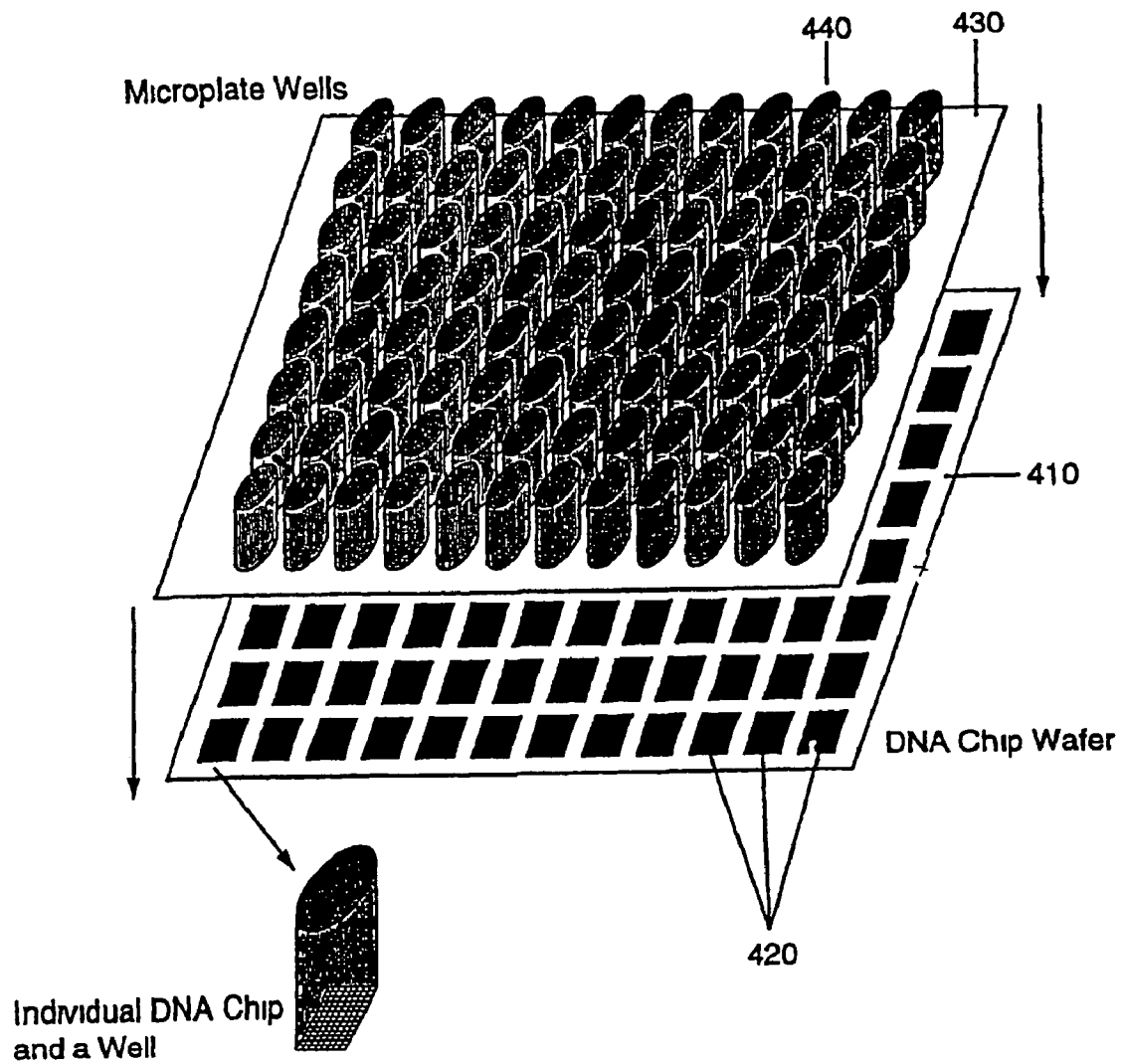


Figure 4

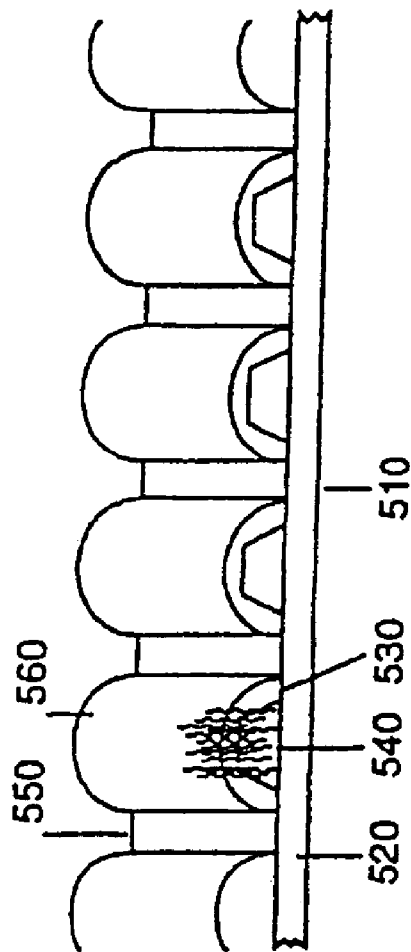


Figure 5

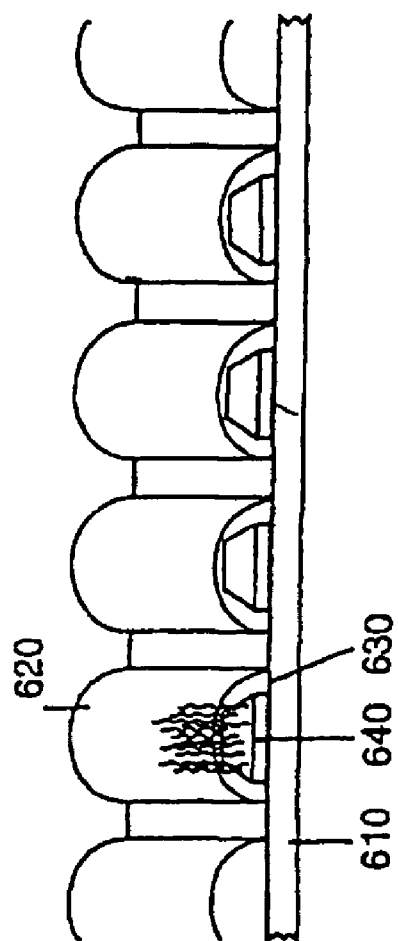


Figure 6

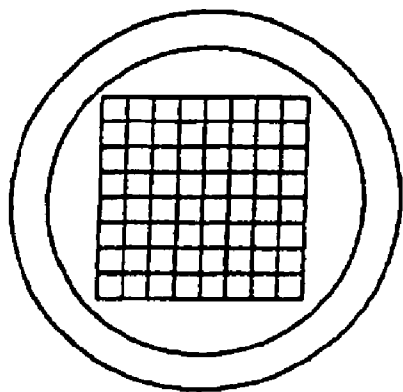


Figure 7

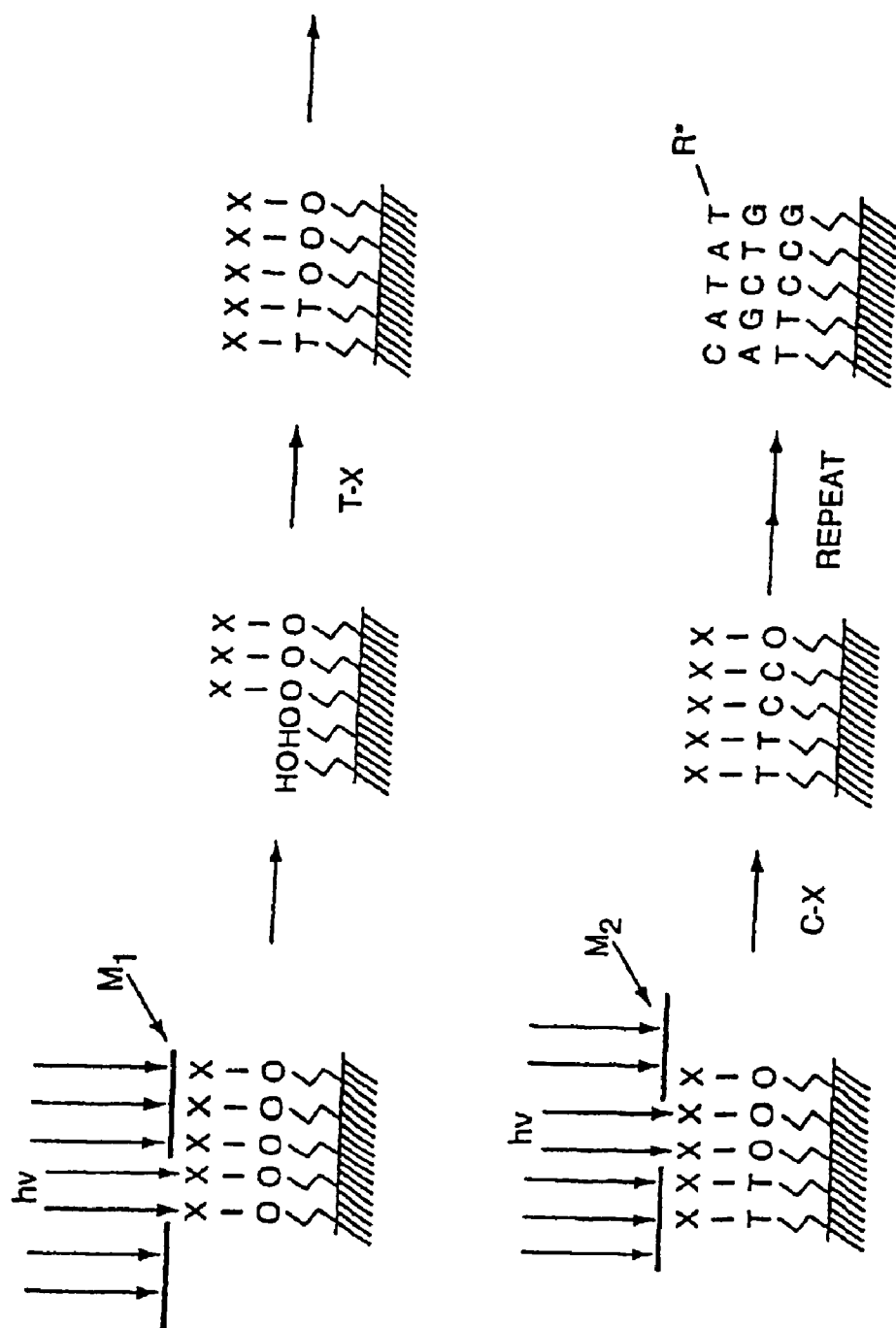


Figure 8

METHODS FOR MAKING A DEVICE FOR CONCURRENTLY PROCESSING MULTIPLE BIOLOGICAL CHIP ASSAYS

RELATED APPLICATIONS

[0001] This application is a continuation of U.S. application Ser. No. 10/157,252, filed May 28, 2002 which is a continuation of Ser. No. 09/247,430, filed Feb. 10, 1999 (now abandoned), which is a continuation of U.S. application Ser. No. 08/630,051, filed Apr. 9, 1996, now U.S. Pat. No. 5,874,219, which is a continuation of U.S. application Ser. No. 08/476,850, filed Jun. 7, 1995, now U.S. Pat. No. 5,545,531. The entire teachings of the above applications are incorporated herein by reference.

BACKGROUND OF THE INVENTION

[0002] This invention relates to methods for concurrently performing multiple biological chip assays. The invention therefore relates to diverse fields impacted by the nature of molecular interaction, including chemistry, biology, medicine and diagnostics.

[0003] New technology, called VLSIPS™, has enabled the production of chips smaller than a thumbnail that contain hundreds of thousands or more of different molecular probes. These biological chips or arrays have probes arranged in arrays, each probe assigned a specific location. Biological chips have been produced in which each location has a scale of, for example, ten microns. The chips can be used to determine whether target molecules interact with any of the probes on the chip. After exposing the array to target molecules under selected test conditions, scanning devices can examine each location in the array and determine whether a target molecule has interacted with the probe at that location.

[0004] Biological chips or arrays are useful in a variety of screening techniques for obtaining information about either the probes or the target molecules. For example, a library of peptides can be used as probes to screen for drugs. The peptides can be exposed to a receptor, and those probes that bind to the receptor can be identified.

[0005] Arrays of nucleic acid probes can be used to extract sequence information from, for example, nucleic acid samples. The samples are exposed to the probes under conditions that allow hybridization. The arrays are then scanned to determine to which probes the sample molecules have hybridized. One can obtain sequence information by careful probe selection and using algorithms to compare patterns of hybridization and non-hybridization. This method is useful for sequencing nucleic acids, as well as sequence checking. For example, the method is useful in diagnostic screening for genetic diseases or for the presence and/or identity of a particular pathogen or a strain of pathogen. For example, there are various strains of HIV, the virus that causes AIDS. Some of them have become resistant to current AIDS therapies. Diagnosticians can use DNA arrays to examine a nucleic acid sample from the virus to determine what strain it belongs to.

[0006] Currently, chips are treated individually, from the step of exposure to the target molecules to scanning. These methods yield exquisitely detailed information. However, they are not adapted for handling multiple samples simul-

aneously. The ability to do so would be advantageous in settings in which large amounts of information are required quickly, such as in clinical diagnostic laboratories or in large-scale undertakings such as the Human Genome Project.

SUMMARY OF THE INVENTION

[0007] This invention provides methods for concurrently processing multiple biological chip assays. According to the methods, a biological chip plate comprising a plurality of test wells is provided. Each test well defines a space for the introduction of a sample and contains a biological array. The array is formed on a surface of the substrate, with the probes exposed to the space. A fluid handling device manipulates the plates to perform steps to carry out reactions between the target molecules in samples and the probes in a plurality of test wells. The biological chip plate is then interrogated by a biological chip plate reader to detect any reactions between target molecules and probes in a plurality of the test wells, thereby generating results of the assay. In a further embodiment of the invention, the method also includes processing the results of the assay with a computer. Such analysis is useful when sequencing a gene by a method that uses an algorithm to process the results of many hybridization assays to provide the nucleotide sequence of the gene.

[0008] The methods of the invention can involve the binding of tagged target molecules to the probes. The tags can be, for example, fluorescent markers, chemiluminescent markers, light scattering markers or radioactive markers. In certain embodiments, the probes are nucleic acids, such as DNA or RNA molecules. The methods can be used to detect or identify a pathogenic organism, such as HIV, or to detect a human gene variant, such as the gene for a genetic disease such as cystic fibrosis, diabetes, muscular dystrophy or predisposition to certain cancers.

[0009] This invention also provides systems for performing the methods of this invention. The systems include a biological chip plate, a fluid handling device that automatically performs steps to carry out assays on samples introduced into a plurality of the test wells, a biological chip plate reader that determines in a plurality of the test wells the results of the assay and, optionally, a computer comprising a program for processing the results. The fluid handling device and plate reader can have a heater/cooler controlled by a thermostat for controlling the temperature of the samples in the test wells and robotically controlled pipets for adding or removing fluids from the test wells at predetermined times.

[0010] In certain embodiments, the probes are attached by light-directed probe synthesis. The biological chip plates can have 96 wells arranged in 8 rows and 12 columns, such as a standard microtiter plate. The probe arrays can each have at least about 100, 1000, 100,000 or 1,000,000 addressable features (e.g., probes). A variety of probes can be used on the plates, including, for example, various polymers such as peptides or nucleic acids.

[0011] The plates can have wells in which the probe array in each test well is the same. Alternatively, when each of several samples are to be subjected to several tests, each row can have the same probe array and each column can have a different array. Alternatively, all the wells can have different arrays.

[0012] Several methods of making biological chip plates are contemplated. In one method, a wafer and a body are provided. The wafer includes a substrate and a surface to which is attached a plurality of arrays of probes. The body has a plurality of channels. The body is attached to the surface of the wafer whereby the channels each cover an array of probes and the wafer closes one end of a plurality of the channels, thereby forming test wells defining spaces for receiving samples. In a second method, a body having a plurality of wells defining spaces is provided and biological chips are provided. The chips are attached to the wells so that the probe arrays are exposed to the space. Another embodiment involves providing a wafer having a plurality of probe arrays; and applying a material resistant to the flow of a liquid sample so as to surround the probe arrays, thereby creating test wells.

[0013] This invention also provides a wafer for making a biological chip plate. The wafer has a substrate and a surface to which are attached a plurality of probe arrays. The probe arrays are arranged on the wafer surface in rows and columns, wherein the probe arrays in each row are the same and the probe arrays in each column are different.

BRIEF DESCRIPTION OF THE DRAWINGS

[0014] FIG. 1 depicts a system of this invention having a biological chip plate, fluid handling device, biological chip plate reader and computer;

[0015] FIG. 2 depicts the scanning of a biological chip plate by a biological chip plate reader,

[0016] FIG. 3 depicts a biological plate of this invention,

[0017] FIG. 4 depicts the mating of a wafer containing many biological arrays with a body having channels to create a biological chip plate,

[0018] FIG. 5 depicts a biological chip plate in cross section having a body attached to a wafer to create closed test wells in which a probe array is exposed to the space in the test well;

[0019] FIG. 6 depicts a biological plate in cross section having a body which has individual biological chips attached to the bottom of the wells;

[0020] FIG. 7 is a top-down view of a test well containing a biological array; and

[0021] FIG. 8 depicts a method of producing an array of oligonucleotide probes on the surface of a substrate by using a mask to expose certain parts of the surface to light, thereby removing photoremovable protective groups, and attaching nucleotides to the exposed reactive groups.

DETAILED DESCRIPTION OF THE INVENTION

[0022] I Definitions

[0023] The following terms are intended to have the following general meanings as they are used herein

[0024] A Complementary: Refers to the topological compatibility or matching together of interacting surfaces of a probe molecule and its target. Thus, the target and its probe can be described as complemen-

tary, and furthermore, the contact surface characteristics are complementary to each other

[0025] B. Probe A probe is a surface-immobilized molecule that can be recognized by a particular target. Examples of probes that can be investigated by this invention include, but are not restricted to, agonists and antagonists for cell membrane receptors, toxins and venoms, viral epitopes, hormones (e.g., opioid peptides, steroids, etc), hormone receptors, peptides, enzymes, enzyme substrates, cofactors, drugs, lectins, sugars, oligonucleotides, nucleic acids, oligosaccharides, proteins, and monoclonal antibodies

[0026] C. Target: A molecule that has an affinity for a given probe. Targets may be naturally-occurring or man-made molecules. Also, they can be employed in their unaltered state or as aggregates with other species. Targets may be attached, covalently or non-covalently, to a binding member, either directly or via a specific binding substance. Examples of targets which can be employed by this invention include, but are not restricted to, antibodies, cell membrane receptors, monoclonal antibodies and antisera reactive with specific antigenic determinants (such as on viruses, cells or other materials), drugs, oligonucleotides, nucleic acids, peptides, cofactors, lectins, sugars, polysaccharides, cells, cellular membranes, and organelles. Targets are sometimes referred to in the art as anti-probes. As the term targets is used herein, no difference in meaning is intended. A "Probe Target Pair" is formed when two macromolecules have combined through molecular recognition to form a complex.

[0027] D. Array A collection of probes, at least two of which are different, arranged in a spatially defined and physically addressable manner

[0028] E. Biological Chip A substrate having a surface to which one or more arrays of probes is attached. The substrate can be, merely by way of example, silicon or glass and can have the thickness of a glass microscope slide or a glass cover slip. Substrates that are transparent to light are useful when the method of performing an assay on the chip involves optical detection. As used herein, the term also refers to a probe array and the substrate to which it is attached that form part of a wafer

[0029] F. Wafer: A substrate having a surface to which a plurality of probe arrays are attached. On a wafer, the arrays are physically separated by a distance of at least about a millimeter, so that individual chips can be made by dicing a wafer or otherwise physically separating the array into units having a probe array.

[0030] G. Biological Chip Plate: A device having an array of biological chips in which the probe array of each chip is separated from the probe array of other chips by a physical barrier resistant to the passage of liquids and forming an area or space, referred to as a "test well," capable of containing liquids in contact with the probe array.

[0031] II General

[0032] This invention provides automated methods for concurrently processing multiple biological chip assays. Currently available methods utilize each biological chip assay individually. The methods of this invention allow many tests to be set up and processed together. Because they allow much higher throughput of test samples, these methods greatly improve the efficiency of performing assays on biological chips.

[0033] In the methods of this invention, a biological chip plate is provided having a plurality of test wells. Each test well includes a biological chip. Test samples, which may contain target molecules, are introduced into the test wells. A fluid handling device exposes the test wells to a chosen set of reaction conditions by, for example, adding or removing fluid from the wells, maintaining the liquid in the wells at predetermined temperatures, and agitating the wells as required, thereby performing the test. Then, a biological chip reader interrogates the probe arrays in the test wells, thereby obtaining the results of the tests. A computer having an appropriate program can further analyze the results from the tests.

[0034] Referring to **FIG. 1**, one embodiment of the invention is a system for concurrently processing biological chip assays. The system includes a biological chip plate reader **100**, a fluid handling device **110**, a biological chip plate **120** and, optionally, a computer **130**. In operation, samples are placed in wells on the chip plate **120** with fluid handling device **110**. The plate optionally can be moved with a stage translation device **140**. Reader **100** is used to identify where targets in the wells have bound to complementary probes. The system operates under control of computer **130** which may optionally interpret the results of the assay.

[0035] A. Biological Chip Plate Reader

[0036] In assays performed on biological chips, detectably labeled target molecules bind to probe molecules. Reading the results of an assay involves detecting a signal produced by the detectable label. Reading assays on a biological chip plate requires a biological chip reader. Accordingly, locations at which target(s) bind with complementary probes can be identified by detecting the location of the label. Through knowledge of the characteristics/sequence of the probe versus location, characteristics of the target can be determined. The nature of the biological chip reader depends upon the particular type of label attached to the target molecules.

[0037] The interaction between targets and probes can be characterized in terms of kinetics and thermodynamics. As such, it may be necessary to interrogate the array while in contact with a solution of labeled targets. In such systems, the detection system must be extremely selective, with the capacity to discriminate between surface-bound and solution-born targets. Also, in order to perform a quantitative analysis, the high-density of the probe sequences requires the system to have the capacity to distinguish between each feature site. The system also should have sensitivity to low signal and a large dynamic range.

[0038] In one embodiment, the chip plate reader includes a confocal detection device having a monochromatic or polychromatic light source, a focusing system for directing an excitation light from the light source to the substrate, a

temperature controller for controlling the substrate temperature during a reaction, and a detector for detecting fluorescence emitted by the targets in response to the excitation light. The detector for detecting the fluorescent emissions from the substrate, in some embodiments, includes a photomultiplier tube. The location to which light is directed may be controlled by, for example, an x-y-z translation table. Translation of the x-y-z table, temperature control, and data collection are managed and recorded by an appropriately programmed digital computer.

[0039] Further details for methods of detecting fluorescently labelled materials on biological chips are provided in U.S. patent application Ser. No. 08/195,889, filed Feb. 10, 1994 and incorporated herein by reference.

[0040] **FIG. 2** illustrates the reader according to one specific embodiment. The chip plate reader comprises a body **200** for immobilizing the biological chip plate. Excitation radiation, from an excitation source **210** having a first wavelength, passes through excitation optics **220** from below the array. The light passes through the chip plate since it is transparent to at least this wavelength of light. The excitation radiation excites a region of a probe array on the biological chip plate **230**. In response, labeled material on the sample emits radiation which has a wavelength that is different from the excitation wavelength. Collection optics **240**, also below the array, then collect the emission from the sample and image it onto a detector **250**, which can house a CCD array, as described below. The detector generates a signal proportional to the amount of radiation sensed thereon. The signals can be assembled to represent an image associated with the plurality of regions from which the emission originated.

[0041] According to one embodiment, a multi-axis translation stage **260** moves the biological chip plate to position different wells to be scanned, and to allow different probe portions of a probe array to be interrogated. As a result, a 2-dimensional image of the probe arrays in each well is obtained.

[0042] The biological chip reader can include auto-focusing feature to maintain the sample in the focal plane of the excitation light throughout the scanning process. Further, a temperature controller may be employed to maintain the sample at a specific temperature while it is being scanned. The multi-axis translation stage, temperature controller, auto-focusing feature, and electronics associated with imaging and data collection are managed by an appropriately programmed digital computer **270**.

[0043] In one embodiment, a beam is focused onto a spot of about $2\ \mu\text{m}$ in diameter on the surface of the plate using, for example, the objective lens of a microscope or other optical means to control beam diameter. (See, e.g., U.S. patent application Ser. No. 08/195,889, *supra*)

[0044] In another embodiment, fluorescent probes are employed in combination with CCD imaging systems. Details of this method are described in U.S. application Ser. No. 08/301,051, incorporated herein by reference in its entirety. In many commercially available microplate readers, typically the light source is placed above a well, and a photodiode detector is below the well. In the present invention, the light source can be replaced with a higher power lamp or laser. In one embodiment, the standard absorption

geometry is used, but the photodiode detector is replaced with a CCD camera and imaging optics to allow rapid imaging of the well. A series of Raman holographic or notch filters can be used in the optical path to eliminate the excitation light while allowing the emission to pass to the detector. In a variation of this method, a fiber optic imaging bundle is utilized to bring the light to the CCD detector. In another embodiment, the laser is placed below the biological chip plate and light directed through the transparent wafer or base that forms the bottom of the biological chip plate. In another embodiment, the CCD array is built into the wafer of the biological chip plate.

[0045] The choice of the CCD array will depend on the number of probes in each biological array. If 2500 probes nominally arranged in a square (50×50) are examined, and 6 lines in each feature are sampled to obtain a good image, then a CCD array of 300×300 pixels is desirable in this area. However, if an individual well has 48,400 probes (220×220) then a CCD array with 1320×1320 pixels is desirable. CCD detectors are commercially available from, e.g., Princeton Instruments, which can meet either of these requirements.

[0046] In another embodiment, the detection device comprises a line scanner, as described in U.S. patent application Ser. No. 08/301,051, filed Sep. 2, 1994, incorporated herein by reference. Excitation optics focuses excitation light to a line at a sample, simultaneously scanning or imaging a strip of the sample. Surface bound labeled targets from the sample fluoresce in response to the light. Collection optics image the emission onto a linear array of light detectors. By employing confocal techniques, substantially only emission from the light's focal plane is imaged. Once a strip has been scanned, the data representing the 1-dimensional image are stored in the memory of a computer. According to one embodiment, a multi-axis translation stage moves the device at a constant velocity to continuously integrate and process data. Alternatively, galvanometric scanners or rotating polyhedral mirrors may be employed to scan the excitation light across the sample. As a result, a 2-dimensional image of the sample is obtained.

[0047] In another embodiment, collection optics direct the emission to a spectrograph which images an emission spectrum onto a 2-dimensional array of light detectors. By using a spectrograph, a full spectrally resolved image of the sample is obtained.

[0048] The read time for a full microtiter plate will depend on the photophysics of the fluorophore (i.e. fluorescence quantum yield and photodestruction yield) as well as the sensitivity of the detector. For fluorescein, sufficient signal-to-noise to read a chip image with a CCD detector can be obtained in about 30 seconds using 3 mW/cm² and 488 nm excitation from an Ar ion laser or lamp. By increasing the laser power, and switching to dyes such as CY3 or CY5 which have lower photodestruction yields and whose emission more closely matches the sensitivity maximum of the CCD detector, one easily is able to read each well in less than 5 seconds. Thus, an entire plate could be examined quantitatively in less than 10 minutes, even if the whole plate has over 4.5 million probes.

[0049] A computer can transform the data into another format for presentation. Data analysis can include the steps of determining, e.g., fluorescent intensity as a function of substrate position from the data collected, removing "outliers"

(data deviating from a predetermined statistical distribution), and calculating the relative binding affinity of the targets from the remaining data. The resulting data can be displayed as an image with color in each region varying according to the light emission or binding affinity between targets and probes therein.

[0050] One application of this system when coupled with the CCD imaging system that speeds performance of the tests is to obtain results of the assay by examining the on- or off-rates of the hybridization. In one embodiment of this method, the amount of binding at each address is determined at several time points after the probes are contacted with the sample. The amount of total hybridization can be determined as a function of the kinetics of binding based on the amount of binding at each time point. Thus, it is not necessary to wait for equilibrium to be reached. The dependence of the hybridization rate for different oligonucleotides on temperature, sample agitation, washing conditions (e.g. pH, solvent characteristics, temperature) can easily be determined in order to maximize the conditions for rate and signal-to-noise. Alternative methods are described in Fodor et al., U.S. Pat. No. 5,324,633, incorporated herein by reference.

[0051] B. Fluid Handling Instruments And Assay Automation

[0052] Assays on biological arrays generally include contacting a probe array with a sample under the selected reaction conditions, optionally washing the well to remove unreacted molecules, and analyzing the biological array for evidence of reaction between target molecules and the probes. These steps involve handling fluids. The methods of this invention automate these steps so as to allow multiple assays to be performed concurrently. Accordingly, this invention employs automated fluid handling systems for concurrently performing the assay steps in each of the test wells. Fluid handling allows uniform treatment of samples in the wells. Microtiter robotic and fluid-handling devices are available commercially, for example, from Tecan AG.

[0053] The plate is introduced into a holder in the fluid-handling device. This robotic device is programmed to set appropriate reaction conditions, such as temperature, add samples to the test wells, incubate the test samples for an appropriate time, remove unreacted samples, wash the wells, add substrates as appropriate and perform detection assays. The particulars of the reaction conditions depends upon the purpose of the assay. For example, in a sequencing assay involving DNA hybridization, standard hybridization conditions are chosen. However, the assay may involve testing whether a sample contains target molecules that react to a probe under a specified set of reaction conditions. In this case, the reaction conditions are chosen accordingly.

[0054] C Biological Chip Plates

[0055] FIG. 3 depicts an example of a biological chip plate 300 used in the methods of this invention based on the standard 96-well microtiter plate in which the chips are located at the bottom of the wells. Biological chip plates include a plurality of test wells 310, each test well defining an area or space for the introduction of a sample, and each test well comprising a biological chip 320, i.e., a substrate and a surface to which an array of probes is attached, the probes being exposed to the space. FIG. 7 shows a top-down view of a well of a biological chip plate of this invention containing a biological chip on the bottom surface of the well.

[0056] This invention contemplates a number of embodiments of the biological chip plate. In a preferred embodiment, depicted in FIG. 4, the biological chip plate includes two parts. One part is a wafer 410 that includes a plurality of biological arrays 420. The other part is the body of the plate 430 that contains channels 440 that form the walls of the well, but that are open at the bottom. The body is attached to the surface of the wafer so as to close one end of the channels, thereby creating wells. The walls of the channels are placed on the wafer so that each surrounds and encloses the probe array of a biological array. FIG. 5 depicts a cross-section of this embodiment, showing the wafer 510 having a substrate 520 (preferably transparent to light) and a surface 530 to which is attached an array of probes 540. A channel wall 550 covers a probe array on the wafer, thereby creating well spaces 560. The wafer can be attached to the body by any attachment means known in the art, for example, gluing (e.g. by ultraviolet-curing epoxy or various sticking tapes), acoustic welding, sealing such as vacuum or suction sealing, or even by relying on the weight of the body on the wafer to resist the flow of fluids between test wells.

[0057] In another preferred embodiment, depicted in cross section in FIG. 6, the plates include a body 610 having pre-formed wells 620, usually flat-bottomed. Individual biological chips 630 are attached to the bottom of the wells so that the surface containing the array of probes 640 is exposed to the well space where the sample is to be placed.

[0058] In another embodiment, the biological chip plate has a wafer having a plurality of probe arrays and a material resistant to the flow of a liquid sample that surrounds each probe array. For example, in an embodiment useful for testing aqueous-based samples, the wafer can be scored with waxes, tapes or other hydrophobic materials in the spaces between the arrays, forming cells that act as test wells. The cells thus contain liquid applied to an array by resisting spillage over the barrier and into another cell. If the sample contains a non-aqueous solvent, such as an alcohol, the material is selected to be resistant to corrosion by the solvent.

[0059] The microplates of this invention have a plurality of test wells that can be arrayed in a variety of ways. In one embodiment, the plates have the general size and shape of standard-sized microtiter plates having 96 wells arranged in an 8x12 format. One advantage of this format is that instrumentation already exists for handling and reading assays on microtiter plates. Therefore, using such plates in biological chip assays does not involve extensive re-engineering of commercially available fluid handling devices. However, the plates can have other formats as well.

[0060] The material from which the body of the biological chip plate is made depends upon the use to which it is to be put. In particular, this invention contemplates a variety of polymers already used for microtiter plates including, for example, (poly)tetrafluoroethylene, (poly)vinylidenedifluoride, polypropylene, polystyrene, polycarbonate, or combinations thereof. When the assay is to be performed by sending an excitation beam through the bottom of the plate collecting data through the bottom of the plate, the body of the plate and the substrate of the chip should be transparent to the wavelengths of light being used.

[0061] The arrangement of probe arrays in the wells of a microplate depends on the particular application contem-

plated. For example, for diagnostic uses involving performing the same test on many samples, every well can have the same array of probes. If several different tests are to be performed on each sample, each row of the plate can have the same array of probes and each column can contain a different array. Samples from a single patient are introduced into the wells of a particular column. Samples from a different patient are introduced into the wells of a different column. In still another embodiment, multiple patient samples are introduced into a single well. If a well indicates a "positive" result for a particular characteristic, the samples from each patient are then rerun, each in a different well, to determine which patient sample gave a positive result.

[0062] D. Biological Chips

[0063] The biological chip plates used in the methods of this invention include biological chips. The array of probe sequences can be fabricated on the biological chip according to the pioneering techniques disclosed in U.S. Pat. No. 5,143,854, PCT WO 92/10092, PCT WO 90/15070, or U.S. application Ser. Nos. 08/249,188, 07/624,120, and 08/082,937, incorporated herein by reference for all purposes. The combination of photolithographic and fabrication techniques may, for example, enable each probe sequence ("feature") to occupy a very small area ("site" or "location") on the support. In some embodiments, this feature site may be as small as a few microns or even a single molecule. For example, a probe array of 0.25 mm² (about the size that would fit in a well of a typical 96-well microtiter plate) could have at least 10, 100, 1000, 10⁴, 10⁵ or 10⁶ features. In an alternative embodiment, such synthesis is performed according to the mechanical techniques disclosed in U.S. Pat. No. 5,384,261, incorporated herein by reference.

[0064] Referring to FIG. 8, in general, linker molecules, $\text{O}-\text{X}$, are provided on a substrate. The substrate is preferably flat but may take on a variety of alternative surface configurations. For example, the substrate may contain raised or depressed regions on which the probes are located. The substrate and its surface preferably form a rigid support on which the sample can be formed. The substrate and its surface are also chosen to provide appropriate light-absorbing characteristics. For instance, the substrate may be functionalized glass, Si, Ge, GaAs, GaP, SiO₂, SiN₄, modified silicon, or any one of a wide variety of gels or polymers such as (poly)tetrafluoroethylene, (poly)vinylidenedifluoride, polystyrene, polycarbonate, polypropylene, or combinations thereof. Other substrate materials will be readily apparent to those of skill in the art upon review of this disclosure. In a preferred embodiment the substrate is flat glass or silica.

[0065] Surfaces on the solid substrate usually, though not always, are composed of the same material as the substrate. Thus, the surface may be composed of any of a wide variety of materials, for example, polymers, plastics, resins, polysaccharides, silica or silica-based materials, carbon, metals, inorganic glasses, membranes, or any of the above-listed substrate materials. In one embodiment, the surface will be optically transparent and will have surface Si—OH functionalities, such as those found on silica surfaces.

[0066] A terminal end of the linker molecules is provided with a reactive functional group protected with a photoremovable protective group, $\text{O}-\text{X}$. Using lithographic methods, the photoremovable protective group is exposed to light, $h\nu$, through a mask, M_1 , that exposes a selected portion

of the surface, and removed from the linker molecules in first selected regions. The substrate is then washed or otherwise contacted with a first monomer that reacts with exposed functional groups on the linker molecules ($-T-X$). In the case of nucleic acids, the monomer can be a phosphoramidite activated nucleoside protected at the 5'-hydroxyl with a photolabile protecting group.

[0067] A second set of selected regions, thereafter, exposed to light through a mask, M_2 , and photoremovable protective group on the linker molecule/protected amino acid or nucleotide is removed at the second set of regions. The substrate is then contacted with a second monomer containing a photoremovable protective group for reaction with exposed functional groups. This process is repeated to selectively apply monomers until polymers of a desired length and desired chemical sequence are obtained. Photolabile groups are then optionally removed and the sequence is, thereafter, optionally capped. Side chain protective groups, if present, are also removed.

[0068] The general process of synthesizing probes by removing protective groups by exposure to light, coupling monomer units to the exposed active sites, and capping unreacted sites is referred to herein as "light-directed probe synthesis." If the probe is an oligonucleotide, the process is referred to as "light-directed oligonucleotide synthesis" and so forth.

[0069] The probes can be made of any molecules whose synthesis involves sequential addition of units. This includes polymers composed of a series of attached units and molecules bearing a common skeleton to which various functional groups are added. Polymers useful as probes in this invention include, for example, both linear and cyclic polymers of nucleic acids, polysaccharides, phospholipids, and peptides having either α -, β -, or ω -amino acids, heteropolymers in which a known drug is covalently bound to any of the above, polyurethanes, polyesters, polycarbonates, polyureas, polyamides, polyethyleneimines, polyarylene sulfides, polysiloxanes, polyimides, polyacetates, or other polymers which will be apparent upon review of this disclosure. Molecules bearing a common skeleton include benzodiazepines and other small molecules, such as described in U.S. Pat. No. 5,288,514, incorporated herein by reference.

[0070] Preferably, probes are arrayed on a chip in addressable rows and columns in which the dimensions of the chip conform to the dimension of the plate test well. Technologies already have been developed to read information from such arrays. The amount of information that can be stored on each plate of chips depends on the lithographic density which is used to synthesize the wafer. For example, if each feature size is about 100 microns on a side, each array can have about 10,000 probe addresses in a 1 cm² area. A plate having 96 wells would contain about 192,000 probes. However, if the arrays have a feature size of 20 microns on a side, each array can have close to 50,000 probes and the plate would have over 4,800,000 probes.

[0071] The selection of probes and their organization in an array depends upon the use to which the biological chip will be put. In one embodiment, the chips are used to sequence or re-sequence nucleic acid molecules, or compare their sequence to a referent molecule. Re-sequencing nucleic acid molecules involves determining whether a particular molecule has any deviations from the sequence of reference molecule. For example, in one embodiment, the plates are used to identify in a particular type of HIV in a set of patient

samples. Tiling strategies for sequence checking of nucleic acids are described in U.S. patent application Ser. No. 08/284,064 (PCT/US94/12305), incorporated herein by reference.

[0072] In typical diagnostic applications, a solution containing one or more targets to be identified (i.e., samples from patients) contacts the probe array. The targets will bind or hybridize with complementary probe sequences. Accordingly, the probes will be selected to have sequences directed to (i.e., having at least some complementarity with) the target sequences to be detected, e.g., human or pathogen sequences. Generally, the targets are tagged with a detectable label. The detectable label can be, for example, a luminescent label, a light scattering label or a radioactive label. Accordingly, locations at which targets hybridize with complementary probes can be identified by locating the markers. Based on the locations where hybridization occurs, information regarding the target sequences can be extracted. The existence of a mutation may be determined by comparing the target sequence with the wild type.

[0073] In a preferred embodiment, the detectable label is a luminescent label. Useful luminescent labels include fluorescent labels, chemi-luminescent labels, bio-luminescent labels, and colorimetric labels, among others. Most preferably, the label is a fluorescent label such as fluorescein, rhodamine, cyanine and so forth. Fluorescent labels include, inter alia, the commercially available fluorescein phosphoramidites such as Fluoreprime (Pharmacia), Fluoredate (Millipore) and FAM (ABI). For example, the entire surface of the substrate is exposed to the activated fluorescent phosphoramidite, which reacts with all of the deprotected 5'-hydroxyl groups. Then the entire substrate is exposed to an alkaline solution (e.g., 50% ethylenediamine in ethanol for 1-2 hours at room temperature). This is necessary to remove the protecting groups from the fluorescein tag.

[0074] To avoid self-quenching interactions between fluorophores on the surface of a biological chip, the fluorescent tag monomer should be diluted with a non-fluorescent analog of equivalent reactivity. For example, in the case of the fluorescein phosphoramidites noted above, a 1:20 dilution of the reagent with a non-fluorescent phosphoramidite such as the standard 5'-DMT-nucleoside phosphoramidites, has been found to be suitable. Correction for background non-specific binding of the fluorescent reagent and other such effects can be determined by routine testing.

[0075] Useful light scattering labels include large colloids, and especially the metal colloids such as those from gold, selenium and titanium oxide.

[0076] Radioactive labels include, for example, ³²P. This label can be detected by a phosphorimager. Detection of course, depends on the resolution of the imager. Phosphorimagers are available having resolution of 50 microns. Accordingly, this label is currently useful with chips having features of that size.

[0077] E Uses

[0078] The methods of this invention will find particular use wherever high throughput of samples is required. In particular, this invention is useful in clinical settings and for sequencing large quantities of DNA, for example in connection with the Human Genome project.

[0079] The clinical setting requires performing the same test on many patient samples. The automated methods of this invention lend themselves to these uses when the test is one

appropriately performed on a biological chip. For example, a DNA array can determine the particular strain of a pathogenic organism based on characteristic DNA sequences of the strain. The advanced techniques based on these assays now can be introduced into the clinic. Fluid samples from several patients are introduced into the test wells of a biological chip plate and the assays are performed concurrently.

[0080] In some embodiments, it may be desirable to perform multiple tests on multiple patient samples concurrently. According to such embodiments, rows (or columns) of the microtiter plate will contain probe arrays for diagnosis of a particular disease or trait. For example, one row might contain probe arrays designed for a particular cancer, while other rows contain probe arrays for another cancer. Patient samples are then introduced into respective columns (or rows) of the microtiter plate. For example, one column may be used to introduce samples from patient "one," another column for patient "two" etc. Accordingly, multiple diagnostic tests may be performed on multiple patients in parallel. In still further embodiments, multiple patient samples are introduced into a single well. In a particular well indicator the presence of a genetic disease or other characteristic, each patient sample is then individually processed to identify which patient exhibits that disease or trait. For relatively rarely occurring characteristics, further order-of-magnitude efficiency may be obtained according to this embodiment.

[0081] Particular assays that will find use in automation include those designed specifically to detect or identify particular variants of a pathogenic organism, such as HIV. Assays to detect or identify a human or animal gene are also contemplated. In one embodiment, the assay is the detection of a human gene variant that indicates existence of or predisposition to a genetic disease, either from acquired or inherited mutations in an individual DNA. These include genetic diseases such as cystic fibrosis, diabetes, and muscular dystrophy, as well as diseases such as cancer (the P53 gene is relevant to some cancers), as disclosed in U.S. patent application Ser. No. 08/143,312, already incorporated by reference.

[0082] The present invention provides a substantially novel method for performing assays on biological arrays. While specific examples have been provided, the above description is illustrative and not restrictive. Many variations of the invention will become apparent to those of skill in the art upon review of this specification. The scope of the invention should, therefore, be determined not with reference to the above description, but instead should be determined with reference to the appended claims along with their full scope of equivalents.

All publications and patent documents cited in this application are incorporated by reference in their entirety for all purposes to the same extent as if each individual publication or patent document were so individually denoted.

1-31. (canceled)

32. A chemical array apparatus comprising: a breakaway seal applied to a surface of a planar substrate, the breakaway seal surrounding a microarray attached to the substrate surface, wherein a portion of the breakaway seal is removable to create a gap in the breakaway seal.

33. The chemical array apparatus of claim 32, wherein the breakaway seal comprises one or both of a physical seal and a chemical seal.

34. The chemical array apparatus of claim 32, wherein the breakaway seal provides fluid isolation to the microarray.

35. The chemical array apparatus of claim 34, wherein the breakaway seal retains a fluid with the microarray until the gap is created, the gap being created on the portion of the breakaway seal that provides a drainage path for the fluid to a perimeter edge of the planar substrate.

36. The chemical array apparatus of claim 34, wherein the fluidly isolated microarray is from a plurality of microarrays attached to the surface of the substrate, and wherein during an assay of the isolated microarray, the breakaway seal retains a fluid with the isolated microarray, such that a remainder of the plurality of microarrays is unaffected by the assay of the isolated microarray.

37. The chemical array apparatus of claim 32, wherein the microarray is from a plurality of microarrays attached to the surface of the substrate, and wherein the breakaway seal provides the plurality of microarrays fluid isolation from one another.

38. The chemical array apparatus of claim 32, wherein the breakaway seal comprises a plurality of sides, the microarray being surrounded by respective sides of the breakaway seal to provide fluid isolation, the respective sides that surround a microarray comprise one or both of a side shared by an adjacent microarray and a side unshared by an adjacent microarray.

39. The chemical array apparatus of claim 38, wherein the gap is created on a respective side surrounding the microarray that is unshared by an adjacent microarray.

40. The chemical array apparatus of claim 32, wherein the breakaway seal forms a channel or path located between adjacent microarrays on the substrate surface.

41. The chemical array apparatus of claim 32, wherein the microarray is from a plurality of microarrays, the plurality of microarrays being arranged in an array pattern that is spatially addressable, the microarray of the plurality comprising a plurality of a chemical or biochemical polymer attached to the substrate surface in a spatially addressable subarray pattern, the breakaway seal having a grid pattern that corresponds to the array pattern, the grid pattern comprising a plurality of zones, the microarray being surrounded by a respective zone of the breakaway seal.

42. The chemical array apparatus of claim 32, wherein the breakaway seal has physical sidewalls that extend a height from the substrate surface, the height being greater than a height that the microarray extends from the substrate surface, the sidewalls being capable of retaining a fluid with the microarray.

43. The chemical array apparatus of claim 32, wherein the breakaway seal is formed by changing a chemical characteristic of the substrate surface along sides surrounding the microarray, the changed characteristic of the substrate retaining a fluid with the microarray using one or both of a hydrophobic effect and a hydrophilic effect.

44. The chemical array apparatus of claim 32, further comprising: a removable cover extending over and in contact with the breakaway seal to enclose or shield the microarray.

45. The chemical array apparatus of claim 44, wherein the microarray is from a plurality of microarrays attached to the substrate surface in an array pattern, the cover shielding the

plurality of microarrays, the cover optionally being selectively removable in sections to uncover a respective microarray relative to a remainder of the plurality of microarrays, the cover being intact over the remainder of the microarrays when a section of the cover is selectively removed.

46. A system for processing a microarray of a chemical array comprising: a chemical array that comprises a microarray attached to a surface of a planar substrate; a breakaway seal provided on the planar substrate to surround the microarray, wherein a portion of the breakaway seal is removable to create a gap in the breakaway seal; and a removable cover extending over and in contact with the breakaway seal to shield the microarray.

47. The system of claim 46, wherein the microarray is from a plurality of microarrays attached to the substrate surface in a spatially addressable array pattern, the breakaway seal comprising sidewalls in a grid pattern that form zones, the grid pattern corresponding to the array pattern.

48. The system of claim 46, wherein the breakaway seal is dimensioned to reduce contact between the cover and the microarray.

49. The system of claim 46, wherein the removable cover is taut over the breakaway seal to reduce contact between the cover and the microarray.

50. The system of claim 46, wherein the cover is removable by peeling the cover away from the breakaway seal.

51. The system of claim 47, wherein the cover is selective removably from the breakaway seal, such that when a section of the cover is selectively removed to expose a respective microarray, a remainder of the cover that shields a remainder of the plurality of microarrays remains intact and unaffected by the selective removal of the section.

52. The system of claim 51, wherein the selectively removable cover comprises a scored pattern corresponding to the grid pattern of the breakaway seal, such that the section of the cover is selectively removable by separating the section along respective scoring of the scored pattern.

53. The system of claim 52, wherein the section of the cover is further selectively removable by peeling the section away from the breakaway seal.

54. The system of claim 47, wherein the cover comprises a film layer and a grid frame layer, the grid frame layer having a plurality of grid frame units arranged in a frame grid pattern, the frame grid pattern corresponding to the grid pattern of the breakaway seal, the grid frame layer being adjacent and securely attached to the breakaway seal, the film layer overlying the grid frame layer, the film layer being readily separable from the grid frame layer relative to the secure attachment of the grid frame layer to the breakaway seal.

55. The system of claim 54, wherein the film layer comprises scoring in a scored pattern, the scored pattern corresponding to the grid frame pattern, the film layer being selectively separable from the grid frame layer in sections along the scoring, such that when a section of the film layer is removed, the section is peeled from a respective grid frame unit and separated from a remainder of the film layer along a portion of the scoring, the removed section exposing a underlying microarray that is otherwise surrounded by sidewalls of a respective zone of the breakaway seal and the respective grid frame unit, and the remainder of the film layer being unaffected by the removal of the film layer section.

56. The system of claim 47, wherein a zone of the grid pattern surrounds and provides fluid isolation to a respective microarray from other microarrays of the plurality, the removable cover being selectively removable from the zone to provide fluid access to the respective microarray that is otherwise surrounded by respective sidewalls of the breakaway seal, and wherein an unremoved portion of the cover remains intact and provides the other microarrays protection from physical damage and fluid contamination.

57. The system of claim 56, wherein during an assay of the respective microarray, a respective section of the cover is selectively removed from the zone to expose the respective microarray, a fluid deposited on the exposed respective microarray being retained by the respective sidewalls of the zone.

58. The system of claim 57, wherein during the assay of the isolated microarray, the removed cover section is applied over the deposited fluid retained by the respective sidewalls to help shield the fluid during the assay.

59. The system of claim 58, wherein further during the assay, localized pressure is deliberately applied to a sidewall of the respective sidewalls of the zone to create the gap in the breakaway seal, the deposited fluid being released through the created gap.

60. The system of claim 46, wherein the portion of the breakaway seal is removed by deliberately applying localized pressure to a sidewall of the breakaway seal, such that the portion breaks away to create the gap in the sidewall.

61. The system of claim 46, further comprising a fixture having a planar inclined surface and a shelf, the inclined surface and the shelf supporting the chemical array during an assay of the microarray.

62. The system of claim 47, wherein the removable cover is adhered to the breakaway seal using one or more of an adhesive at between the cover and an edge surface of a sidewall of the breakaway seal, an electrostatic attraction between the breakaway seal and the cover along the edge surface of a sidewall, and an adhesive strip in an adhesive grid pattern similar to the breakaway seal grid pattern between the cover and the edge surface of the sidewalls.

63. The system of claim 47, wherein the microarray comprises a plurality of a chemical or biochemical polymer attached to the substrate surface in a spatially addressable subarray pattern.

64. A method of processing a microarray of a chemical array of microarrays comprising: applying a breakaway seal to a surface of a planar substrate to ultimately surround a microarray on the planar substrate; processing the microarray with a fluid that is deposited on the microarray, the breakaway seal retaining the fluid with the microarray; and breaking away a portion of the breakaway seal that retains the fluid with the microarray, the broken away portion creating a gap in the breakaway seal, the gap providing an exit for the release of the fluid from the microarray.

65. The method of claim 64, further comprising attaching a plurality of microarrays to the substrate surface in an array pattern either before or after the breakaway seal is applied, the microarray being from the plurality, the array pattern being spatially addressable, the microarray comprising a plurality of a chemical or biochemical polymer arranged in a subarray pattern that is spatially addressable.

66. The method of claim 64, wherein breaking away a portion of the breakaway seal comprises tilting and orienting

the planar substrate in a direction such that the retained fluid will drain through the gap and off the planar substrate.

67. The method of claim 64, wherein the gap is created in the portion of the breakaway seal facing a perimeter edge of the planar substrate, such that the fluid is released in a direction of the facing perimeter edge off the planar substrate.

68. The method of claim 64, wherein breaking away a portion of the seal comprises: holding the planar substrate at an incline angle, the incline angle being such that the fluid is prevented from exceeding the breakaway seal until the gap is created; orienting the planar substrate such that a perimeter edge of the planar substrate is at a lowest position when inclined, the lowest position of the substrate perimeter edge being relative to other perimeter edges of the planar substrate; and applying localized pressure to a sidewall of the portion of the breakaway seal surrounding the microarray, the gap being created in the sidewall, the fluid exiting through the gap off the planar substrate in the direction of the lowest substrate perimeter edge.

69. The method of claim 68, wherein the incline angle assists the fluid to flow through the gap when created.

70. The method of claim 64, further comprising: covering the microarray with a removable cover, the cover being in contact with the breakaway seal, the cover shielding the microarray; and removing the cover before processing the microarray, the removed cover providing fluid access to the microarray.

71. The method of claim 70, wherein the microarray is from a plurality of microarrays attached to the substrate surface in an array pattern, the cover being selectively removable from the breakaway seal, such that during removing, a section of the removable cover over the microarray is selectively removed before processing, a remainder of the removable cover being intact over the other microarrays, wherein selectively removing the section of the cover provides fluid access to the uncovered microarray while shielding the other microarrays from the fluid.

72. The method of claim 70, further comprising applying the removed cover on the fluid to help shield the fluid during processing.

73. The method of claim 64, further comprising one or more of: rinsing the microarray with a wash solution that drains through the created gap; scanning the microarray using scanning equipment to determine results of the processing; storing the planar substrate until another microarray on the substrate having an intact breakaway seal is to be processed; and processing another microarray on the substrate surrounded by an intact portion of the breakaway seal with another fluid when the processing of the microarray having the created gap in the breakaway seal is complete.

74. A removable cover for a chemical array apparatus comprising a sheet of material that overlies a microarray of the chemical array apparatus, the sheet being removable to provide fluid access to the microarray.

75. The removable cover of claim 74, wherein when the sheet is removed, the microarray is exposed, the removed sheet being reapplied on a fluid deposited on the exposed microarray during an assay, the reapplied sheet helping to shield the fluid during the assay of the microarray.

76. The removable cover of claim 74, wherein the chemical array apparatus comprises an array pattern of microarrays, the sheet overlying the microarrays of the array pattern, the sheet being independently removable from over a respective microarray of the array pattern, such that other microarrays of the chemical array apparatus remain covered.

77. The removable cover of claim 74, wherein the sheet of material is taut over the microarray to reduce contact between the sheet and the microarray.

78. The removable cover of claim 74, wherein the sheet is removable by peeling the sheet away from the chemical array apparatus.

79. The removable cover of claim 76, wherein the sheet is independently removably from the chemical array apparatus in sections, the independently removable sheet comprises a scored pattern corresponding to the array pattern of microarrays, such that a section of the sheet is selectively removed by separating the section along respective scoring of the scored pattern.

80. The removable cover of claim 76, wherein the sheet of material comprises a film layer and a grid frame layer, the grid frame layer having a plurality of grid frame units arranged in a frame grid pattern, the frame grid pattern corresponding to the array pattern of the microarrays, the grid frame layer being adjacent and securely attached to the chemical array apparatus, the film layer overlying the grid frame layer, the film layer being readily separable from the grid frame layer relative to the secure attachment of the grid frame layer to the chemical array apparatus.

81. The removable cover of claim 80, wherein the film layer comprises scoring in a scored pattern, the scored pattern corresponding to the grid frame pattern, the film layer being selectively separable from the grid frame layer in sections along the scoring, such that when a section of the film layer is selectively removed, the section is peeled from a respective grid frame unit and separated from a remainder of the film layer along a portion of the scoring, a remainder of the film layer being unaffected by the removal of the film layer section.

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