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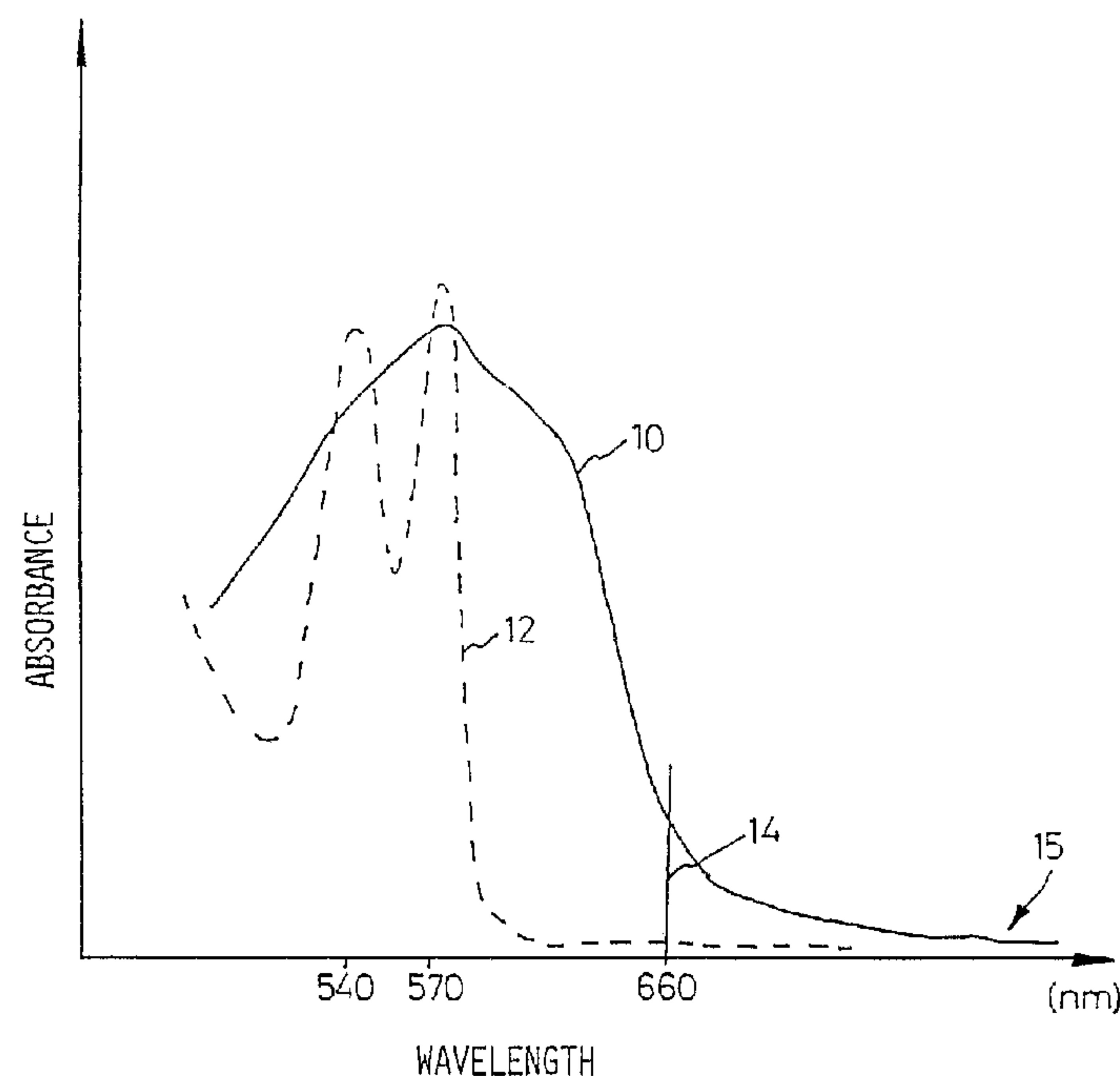
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(54) Titre : METHODE DE DETERMINATION DU GLUCOSE DANS LE SANG TOTAL, CUVE ET PHOTOMETRE POUR CE FAIRE

(54) Title: METHOD FOR DETERMINATION OF GLUCOSE IN WHOLE BLOOD AND CUVETTE AND PHOTOMETER FOR CARRYING OUT SAID METHOD



(57) Abrégé/Abstract:

A sample of whole blood is contacted with a reagent which by chemical reaction with glucose in the sample brings about a detectable dye concentration change (10) the size of which is determined as a measure of the glucose content of the sample. The sample is initially introduced undiluted in a microcuvette having at least one cavity for receiving the sample. The cavity is internally pretreated with the reagent in dry form, and the chemical reaction takes place in the cavity. Active components of the reagent comprise at least a hemolysing agent for exposing glucose contained in the blood cells of the sample for allowing total glucose determination, and agents taking part in the chemical reaction and ensuring that the dye concentration change (10) takes place at least in a wavelength range (14) outside the absorption range (12) of the blood hemoglobin. An absorption measurement is performed in said wavelength range directly on the sample in the cuvette. A pretreated disposable cuvette with such a reagent and a photometer are also described.





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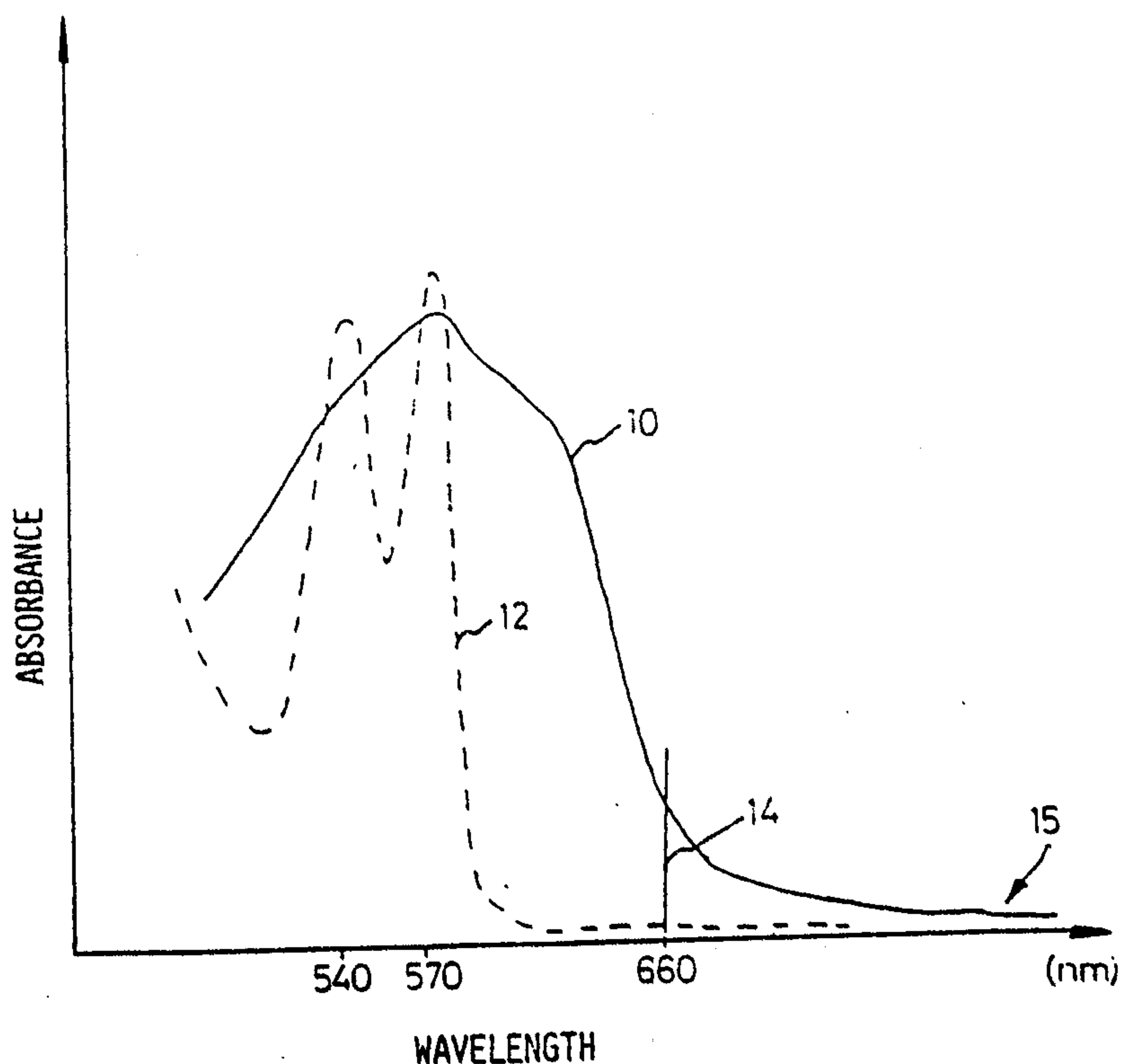
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<b>(21) International Application Number:</b> PCT/SE90/00273 <b>(22) International Filing Date:</b> 24 April 1990 (24.04.90)  <b>(30) Priority data:</b> 8901514-3                      25 April 1989 (25.04.89)                      SE  <b>(71) Applicant (for all designated States except US):</b> MIGRATA UK LTD [GB/GB]; 2 Duke Street, St James's, London SW1 Y6BJ (GB).  <b>(72) Inventors; and</b> <b>(75) Inventors/Applicants (for US only) :</b> LILJA, Jan, Evert [SE/ SE]; Södra Brunnsvägen 63, S-253 68 Helsingborg (SE). NILSSON, Sven-Erik, Lennart [SE/SE]; Döbeliusvägen 39, S-283 67 Helsingborg (SE).		<b>(74) Agent:</b> AWAPATENT AB; Box 5117, S-200 71 Malmö (SE).  <b>(81) Designated States:</b> AT, AT (European patent), AU, BB, BE (European patent), BF (OAPI patent), BG, BJ (OAPI patent), BR, CA, CF (OAPI patent), CG (OAPI patent), + CH, CH (European patent), CM (OAPI patent), DE, + DE (European patent), DK, DK (European patent), ES, ES (European patent), FI, FR (European patent), GA (OAPI patent), GB, GB (European patent), HU, IT (Eu- ropean patent), JP, KP, KR, LK, LU, LU (European pa- tent), MC, MG, ML (OAPI patent), MR (OAPI patent), MW, NL, NL (European patent), NO, RO, SD, SE, SE (European patent), SN (OAPI patent), SU, TD (OAPI patent), TG (OAPI patent), US.  <b>Published</b> <i>With international search report.</i> <i>In English translation (filed in Swedish).</i>

**(54) Title:** METHOD FOR DETERMINATION OF GLUCOSE IN WHOLE BLOOD AND CUVETTE AND PHOTOME-  
TER FOR CARRYING OUT SAID METHOD

**(57) Abstract**

A sample of whole blood is contacted with a reagent which by chemical reaction with glucose in the sample brings about a detectable dye concentration change (10) the size of which is determined as a measure of the glucose content of the sample. The sample is initially introduced undiluted in a microcuvette having at least one cavity for receiving the sample. The cavity is internally pretreated with the reagent in dry form, and the chemical reaction takes place in the cavity. Active components of the reagent comprise at least a hemolysing agent for exposing glucose contained in the blood cells of the sample for allowing total glucose determination, and agents taking part in the chemical reaction and ensuring that the dye concentration change (10) takes place at least in a wavelength range (14) outside the absorption range (12) of the blood hemoglobin. An absorption measurement is performed in said wavelength range directly on the sample in the cuvette. A pretreated disposable cuvette with such a reagent and a photometer are also described.





METHOD FOR DETERMINATION OF GLUCOSE IN WHOLE BLOOD AND  
CUVETTE AND PHOTOMETER FOR CARRYING OUT SAID METHOD

The present invention relates to a method for  
5 quantitatively determining total glucose content in whole  
blood, and to a disposable cuvette and a photometer for  
carrying out the method.

Determination of whole blood glucose is made for  
diagnosing and controlling diabetes, and also in endo-  
10 crinological investigations. In uncertain cases of uncon-  
sciousness, too, determination of whole blood glucose may  
be justified. Diabetes is one of the world's major health  
problems, and it is estimated that more than 40 million  
people suffer from this disease and that the prevalence  
15 of type II diabetes seems to increase.

Several methods for determining glucose are known.  
Many old methods have today been abandoned because of  
unspecificity or the involvement of carcinogenic reagents.

By glucose in blood, whole blood glucose, is meant  
20 non-protein-bound glucose present in the blood. Glucose is  
freely distributed in the extracellular water and also in  
the intracellular water, e.g. in the red blood cells, but  
not necessarily in the same concentration. This means that  
the total content of glucose in whole blood differs from  
25 the total content of glucose in plasma or serum. The  
diagnostic criteria for e.g. diabetes are predominantly  
based on whole blood glucose. To the clinician, it is  
therefore clearly advantageous to have the glucose deter-  
minations made directly on whole blood. The difference  
30 between determinations of glucose in whole blood and  
glucose in plasma or serum is discussed by W.T. Caraway:  
Amer. J. Clin. Path. 37:445, 1962. Many glucose tests  
currently used, where intact red blood cells are removed,  
incorrectly state their results as blood glucose and may  
35 therefore cause confusion in medical diagnosis because of  
the different references used.

Most of today's specific glucose determination methods are based on reagents containing enzymes or enzyme systems. Three different enzyme systems are predominant, viz. glucose oxidase, hexokinase and glucose dehydrogenase (GDH).  
5

The present invention preferably relies on reagents containing glucose dehydrogenase (GDH). Previously known determination methods using GDH are described in US 4,120,755 and US 3,964,974. These prior art determination methods using GDH are traditional wet-chemical methods.  
10

None of the above-mentioned methods is however suitable for determining glucose in undiluted whole blood. Although Example 7 in US 3,964,974 describes a whole blood glucose method, this method is based on dilution and protein precipitation or separate hemolysis of the blood sample.  
15

EP 84112835.8 describes a whole blood glucose method for undiluted blood. The chemical enzyme reaction used is based on glucose oxidase, and an optical reflectance measurement is carried out at a wavelength above 600 nm. It is well known that hemoglobin interferes with oxidase reactions. Also, oxidase reactions require access to free oxygen. Therefore, using a microcuvette for performing a whole blood glucose determination with the glucose oxidase system in undiluted blood involves substantial problems.  
20  
25

From US 4,088,448 is previously known a microcuvette which can be used for hemoglobin measurement (Hb measurement) of blood. The cuvette is pretreated with a reagent, such that when a blood sample is drawn into the cuvette, the walls of the red blood cells are dissolved and a chemical reaction is initiated, the result of which allows Hb determination by absorption measurement directly through the cuvette which, to this end, has an accurately defined gap width.  
30

The method according to US 4,088,448 for Hb determination on glucose is not easily applied in practice since an absorption measurement for determining the  
35



glucose content is strongly interfered with by the absorption caused by the hemoglobin. Variations in the hemoglobin concentration will therefore interfere with the glucose determination to a considerable extent.

5        Thus, present-day methods are complicated. They often require dilution of the blood sample or only perform a glucose determination on the blood plasma without taking into account the glucose contents of the red blood cells.

10       It is therefore evident that a simple, reliable and quick method for quantitatively determining the total content of glucose in undiluted whole blood would be an important aid in diagnosing and controlling diabetes.

15       One object of the present invention is to provide a method for quantitatively determining the total content of glucose in undiluted whole blood by transmission photometry. Another object is to provide a cuvette and a photometer for such determination.

20       Generally, the above-mentioned interference problem caused by the hemoglobin content is solved according to the invention in the following way:

25       By using a suitable reagent, it is possible first to cause the walls of the red blood cells to dissolve, and then to bring about a chemical reaction between the total glucose content of the blood sample and the reagent, which reaction yields chemical compounds which are based on the glucose and the absorption range of which, wavelengthwise, is at least partly outside the wavelength range of the hemoglobin absorption range. Thus, by absorption measurements at suitably selected wavelengths it is possible to  
30       completely eliminate the influence of the hemoglobin on the measuring result and to achieve very quick glucose determination.

35       Thus, the invention provides a method for glucose determination in whole blood, in which a sample of whole blood is contacted with a reagent which by chemical reaction with glucose in the sample brings about a dye concentration change which is detectable in the sample and

the size of which is determined as a measure of the glucose content, the method being characterised by the steps of

introducing the sample undiluted in a microcuvette  
5 having at least one cavity for receiving the sample, said cavity being internally pretreated with the reagent in dry form and said chemical reaction then taking place in said cavity,

selecting as active components included in the  
10 reagent at least a hemolysing agent for exposing glucose contained in the blood cells of the sample for allowing a quantitative total glucose determination in a whole blood hemolysate, and agents participating in the chemical reaction and ensuring that the dye concentration change takes  
15 place at least in a wavelength range outside the absorption range of the blood hemoglobin, and

performing an absorption measurement at said wavelength range directly on the sample in the cuvette.

Preferred embodiments of the inventive method are  
20 stated in the subclaims 2-7.

According to a preferred embodiment of the invention, the method comprises the steps of supplying undiluted whole blood to a dry reagent in a cuvette having a small gap width including a hemolysing agent, GDH, diaphorase or  
25 analog thereof, NAD or analog thereof, detergent and a dye-forming substance, and photometrically measuring the concentration of dye formed by transmission measurement in a filter photometer. Diaphorase analogs are substances having redox properties of the type phenazine mettro-  
30 sulphate or phenazine ettrosulphate. These may replace diaphorase substances, but are unsuitable from the point of view of toxicity.

The glucose dehydrogenase method is specific to  $\beta$ -glucose. In blood,  $\alpha$ -glucose and  $\beta$ -glucose exist in a  
35 temperature-dependent equilibrium. When lowering the temperature of a blood sample, the equilibrium is shifted towards a larger proportion of  $\alpha$ -glucose. The change of



equilibrium is slow. The reaction speed of the glucose dehydrogenase method is affected by the enzyme mutarotase and, thus, the  $\alpha$ -glucose/ $\beta$ -glucose equilibrium. In blood glucose determination, it is essential that the analysis  
5 is carried out without any delay to prevent inherent metabolism in the sample. Since the spontaneous  $\alpha$ - $\beta$  reaction occurs very slowly and the body temperature is sufficiently constant for ensuring the  $\alpha$ / $\beta$  equilibrium, mutarotase can advantageously be excluded in the case of  
10 direct testing on body-temperature blood, yet allowing calibration of the photometer in total glucose. In addition to the cost reduction, the advantages of the method reside in a decreased reaction time and an extended analytical range. A disadvantage is that calibration and  
15 control solutions should be brought to proper temperature during at least 1 h.

According to a preferred embodiment of the invention, a reagent system of the glucose dehydrogenase type consists of a hemolysing agent for breaking up the red blood  
20 cells and liberating hemoglobin, GDH diaphorase or analog to make the NADH reaction visible, NAD or analog, detergent or a dye-forming substance, e.g. taken from the group of tetrazolium compounds. In addition to these active substances, other chemical substances can be used as produc-  
25 tion aids.

The absorbance by the hemoglobin liberated during hemolysis is described in E.J. van Kampen and W.G. Zijlstra (1965): "Determination of hemoglobin and its derivations" in Adv. Clin. Chem. 8, 141-187, p 165, Fig. 12. It is seen  
30 from this figure that in case an absorption measurement occurs at a wavelength above 645 nm, the effect of any hemoglobin derivative is minimised.

Another type of interference in absorption measurements is e.g. particle scattering of the light from cells,  
35 fat, dust or other deficiencies. By measuring at another wavelength, often above the primary measuring wavelength, where neither hemoglobin nor the dye formed gives rise to

any interfering absorbance, this background absorbance can be compensated for.

The reaction process of the glucose dehydrogenase system is well known and described in US 3,964,974. This publication reports on a reaction process comprising  
5 tetrazolium salt with absorption in the visible range.

An essential feature of the method according to the invention is the use of a glucose dehydrogenase reaction proceeding to end-point, both chemically and in respect of  
10 absorption photometry. In terms of safety and reliability, such a reaction is preferable to the user.

Optical methods for quantitative determination of the concentration of a chemical substance in a solution are well known and well documented. Absorption photometry is  
15 an optical determination technique. The theory behind absorption photometry and the design of a photometer are described in Skoog and West: "Fundamentals of Analytical Chemistry", Section Edition, Chapter 29. Basically, a photometer consists of three parts, an optical part, a  
20 mechanical part and an electronic part. The optical part consists of a light source with a monochromator or interference filter and a light detector, and in some cases a lens system. The mechanical part comprises the suspension of the optical part and means for transporting cuvettes  
25 with chemical solution. The electronic part is designed for the control and monitoring of the light source and the measuring signals from light detectors, these signals being so processed that the user can read a numerical value which is related to or represents the chemical con-  
30 centration measured.

Such a photometer construction is disclosed in US 4,357,105. This patent describes a photometer for determining hemoglobin in blood, which provides optimisation with known components, such that the photometric determination occurs as close to the measuring wavelength 540 nm  
35 as possible. The adjustment to the measuring wavelength 540 nm is carried out by using a light emitting diode and



a light filter of the didymium-oxide glass type. In an alternative embodiment, a light emitting diode is used within the infrared range for measuring turbidity in the chemical solution. This known photometer is intended to be  
5 used for ordinary wet-chemical hemoglobin determination methods, having a degree of dilution of 1/200 and above between blood and reagent.

A photometer for determining the glucose content in whole blood according to the method described, i.e.  
10 supplying dry glucose reagent to undiluted blood and performing a photometric two-wavelength measurement on a microcuvette, must be simple, reliable and available at a low cost. Since the cuvette contains a dry glucose reagent, it is of the disposable type, and the transport  
15 of the cuvette, after filling with undiluted blood, must be uncomplicated and minimise the effect of stray light. In terms of operation, the photometer must be photometrically stable and require a minimum of controlling.

20 Thus, in order to carry out the inventive method the invention further provides a disposable cuvette according to claim 8 pretreated with a dry reagent, and a photometer according to claim 9 operating at two separate wavelengths, preferred embodiments of the latter being stated  
25 in claims 10 and 11.

A photometer for carrying out the inventive method for measuring whole blood glucose in small volumes in undiluted blood by means of a microprocessor for monitoring and controlling and having arithmetic calculation  
30 capacity, as well as light emitting diodes provided with an interference filter, gives a construction which is easy to handle, technically stable and employs silicon electronics throughout, has low power consumption, is highly reliable and can be manufactured at a low cost. If the  
35 mechanical part, the outer casing and the bottom as well as the cuvette transport means, including the part where the optical components are attached, is made of injection-

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moulded plastic, the overall production costs for the photometer will be low.

A microprocessor-assisted photometer is able to control all processes and carry out all calculations including logarithmic transformations. The light emitting diodes of a photometer for two-wavelength measurements are pulsed via the microprocessor such that only one light emitting diode is lit at a time. Light emitting diodes are highly advantageous by having no afterglow. In order to ensure that the light emitting diodes do not lose their light intensity by ageing, the photometer is designed such that maximal light intensity, corresponding to 100% light, is regularly measured between different cuvette measurements. By designing the mechanical cuvette transport function such that the photometer can sense if a cuvette should be measured or if the total intensity, 100% light, should be measured, the photometer can operate with a compensation for light intensity. By the possibility of establishing whether the measured value is a cuvette value or a blank value, 100% transmission, the photometer can operate, by means of its microprocessor equipment, without any logarithmic analog amplifiers. The absence of logarithmic analog amplifiers increases the reliability and the stability of the photometer while at the same time arbitrary accuracy in the logarithmic operation is achieved by a logarithmic algorithm in the microprocessor program. A further advantage of a microprocessor-assisted photometer is that different forms of arithmetic curve adaptations of calibration curves or linearisations can easily be introduced in the program. By the microprocessor function, it is also possible to use different forms of end-point routines, i.e. the program can itself decide when the end-point has been reached, which can be done with different accuracies for different concentration levels, where so desirable.



The invention will now be described in more detail with reference to the accompanying drawings.

Fig. 1 is a graph with absorbance set against wavelength, both for a mix of hemoglobin derivatives and for a dye-forming substance included in a glucose reagent.

Figs. 2A, 3A and 4A show three different embodiments of an inventive photometer.

Figs. 2B, 3B and 4B correspond to the embodiments of Figs. 2A, 3A and 4A, respectively, but include a separate logarithmic amplifier.

Fig. 5 schematically shows a broken-apart section of an embodiment of the optical part of an inventive photometer.

Fig. 1 indicates by a full line 10 an absorption spectrum for a tetrazolium salt, 3-(4,5-dimethyl thiazolyl-1-2)-2,5-diphenyl tetrazolium bromide (MTT), and by a dashed line 12 an absorption spectrum for hemolysed blood. It is seen that above 600 nm there is a wavelength range where MTT can be quantitatively determined with a minimum of interference by hemoglobin. It also appears that compensation for background interference can occur at higher wavelengths. At two-wavelength measurements in absorption, it is essential to use wavelengths which are distinctly separated so as not to interfere with each other. The interference filters used in the filter photometer are defined wavelengthwise by the wavelength where maximal light transmission is obtained. In addition, an interference filter has a half bandwidth defined where a maximum of 50% of the light transmission is obtained.

Figs. 2A, 3A, 4A and 2B, 3B, 4B show different embodiments of a microprocessor-assisted photometer. Version 'A' in these Figures shows a photometer without a logarithmic amplifier, the logarithmic operation taking place in the program of the microprocessor. Version 'B' in these Figures makes use of a separate logarithmic amplifier 19. The use of a separate logarithmic amplifier 19

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means simpler programs in the microprocessor, but poorer technical characteristics of the photometer.

Figs. 2A, 2B and 3A, 3B differ in that Figs. 3A, 3B make use of a digital-to-analog converter 46 when passing  
5 from analog to digital form. This arrangement has the advantage of being economical, but gives poorer stability by necessitating peripheral equipment.

The photometer in Figs. 2-4 physically consists of two structural blocks: one optical housing and one elec-  
10 tronic printed circuit board 16. The electronic printed circuit board is of standard type where the components used are applied by surface mounting or soldering in traditional manner in a drilled laminate board. In certain cases, it is possible to use a printed circuit board  
15 allowing a combination of different mounting techniques.

The embodiment in Fig. 2A will now be described in more detail. A printed circuit board 16 included in the photometer is schematically shown by dash-dot lines and contains a microprocessor 18, an analog-to-digital con-  
20 verter 20, a multiplexer 22, a potentiometer 24, an LCD drive unit 26, an LCD display unit 28, a light emitting diode drive circuit 30, a mains rectifier 32, a battery charging circuit 34, and peripheral equipment (not shown) of a type known to a person skilled in the art.

25 The printed circuit board 16 is connected to the other photometer part comprising a cuvette housing 36, two light emitting diodes 38, a light sensor 40, and a switch 42.

In operation, the multiplexer 22 receives analog signals from the light sensor 40, from the battery charg-  
30 ing circuit 34 and from the potentiometer 24 and transmits, in accordance with control instructions 44 from the microprocessor 18, one of these signals to the analog-to-digital converter 20. This converts the signal to a form which can be handled by the processor 18 which depending  
35 on the signal received executes different operations.



The processor 18 receives the signal from the potentiometer 24, which is adjustable by the user, when the photometer is calibrated by means of a sample of known glucose content. In this way, a constant is established in  
5 the algorithm by means of which the glucose content is calculated on the basis of the transmittance measured.

The processor 18 receives the signal from the battery charging circuit 34 when the processor 18 should compensate for varying battery charge.

10 The processor 18 receives the digitilised measuring signal from the light sensor 40, both when measuring 100% transmittance as reference, and when measuring transmittance through the blood sample in a disposable cuvette placed between the light emitting diodes 38 and the light  
15 sensor 40.

On the basis of a preprogrammed algorithm, the processor 18 calculates the glucose content of the sample and emits the result to the LCD drive circuit 26 for displaying it to the user on the LCD display 28.

20 In Figs. 2B, 3A and 3B as well as 4A and 4B, like parts, as in Fig. 2A, are represented by like reference numerals.

In the variant of Fig. 3A, the analog-to-digital converter in Fig. 2A is excluded and replaced by a combination of a comparator 45, a digital-to-analog converter 46  
25 and the microprocessor 18. The processor 18 emits to the converter 46 a digital value which is converted to analog form and which is successively changed by the processor 18 until a zero signal is obtained on the output of the  
30 comparator 45. Otherwise, the function is the same as in Fig. 2A.

The basic design of the optical housing appears from Fig. 5. The arrangement comprises two light emitting diodes 52, 64 disposed at 90° to each other. To obtain a  
35 similar optical axis, the light emitting diodes should be adjusted prior to mounting.

A photometer for glucose in undiluted blood can have its measuring wavelength at 660 nm (at 14 in Fig. 1). As a result of the measurement of the absorbance flank on the dye formed, the half bandwidth of the measuring wavelength must be well defined. The background wavelength for measuring glucose in undiluted blood should be above 700 nm. A suitable choice of background wavelength is where commercial light emitting diodes are available, e.g. 740-940 nm.

In Fig. 5, it is seen how a light ray 50 from a red light emitting diode 52 passes an interference filter 54 having maximal light transmission at 660 nm and a half bandwidth less than 15 nm, and through a mirror disposed at an angle of  $45^\circ$ . After the light ray 50 has passed the interference filter 54 and the mirror 56, it passes through the cavity 60 of the cuvette 58, which cavity contains undiluted whole blood and glucose reagent or glucose reagent products, and reaches the light detector 40 through an opening 53 in a cuvette holder 55. The light detector 40 can be provided with a small collecting lens 62.

The light ray from the infrared light emitting diode 64 is reflected on the rear side of the  $45^\circ$ -inclined mirror 56, passes through the cavity 60 of the cuvette 58 and reaches the detector 40. The infrared background wavelength is measured with the second light emitting diode 64 and on a plane absorbance level (e.g. at 15 in Fig. 1), the half bandwidth of the infrared light emitting diode 64 being of little importance.

If the cuvette transport device 55, e.g. a carriage construction, is equipped with an element that can be sensed by a stationarily arranged sensor, the micro-processor 18 can easily be supplied with information 43 about the position in which the cuvette 58 is situated. If a carriage 55 is used as cuvette conveyor, it may have a magnet which is sensed by two fixed magnetic reed relays. When the carriage is in the extracted position for intro-



ducing the cuvette 58, maximal light, 100% light, is measured.

Maximal light is measured for both measuring wavelength and background measuring wavelength. By continuously  
5 ly calculating the quotient in per cent between measuring value, cuvette in measuring position and maximal light, good compensation for ageing phenomena in the light sources 52, 64 is obtained in transmittance measurement. A logarithmic operation on the transmission value is  
10 executed in the microprocessor 18, or in a separate circuit (see version 'B') for receiving a measure of absorbance.

The current of the light detector 40 reaches an operational amplifier which converts current to voltage to  
15 permit easy processing of the signals on the printed circuit board 16. The microprocessor 18 also monitors whether the dark current from the detector 40 is low and compensates for the influence of the dark current by taking this into account in the calculation formulae used.

20 In Figs. 2-4, there is only one movable part, viz. the potentiometer 24. The potentiometer 24 is the only component which the user can operate on the printed circuit board 16. The potentiometer 24 is used for calibrating the photometer against blood of known glucose  
25 content. To achieve maximal stability, the other components of the photometer are preferably stationary.

For economic reasons, the microprocessor is a one-chip processor. To save energy, the digit displays are of the LCD type and the photometer is supplied with energy  
30 from a mains transformer or a battery.

Fig. 4A shows another embodiment of the invention. This version uses the programming possibilities of the microprocessor 18 for providing a photometer which is easier to trim and has enhanced stability. This is  
35 achieved in that the supply of current to the two light emitting diodes 38 is controlled through a digital-to-analog converter 70 which, in terms of programming, is in

feedback with the measuring signal. It is then possible, in terms of measurement, to maintain the blank value, 100% transmission, on a constant level. This constant level is electronically determined by the resolution (number of  
5 bits) in the digital-to-analog conversion.

### Example

A microcuvette 58 of the type described in the above-  
10 mentioned US 4,088,448 was provided by freeze-drying with a dry reagent for quantitative determination of total glucose in whole blood. The microcuvette was charged with dry reagent by producing, in a first step, a water-soluble reagent composition. The water-soluble glucose reagent  
15 composition consisted of (volume 1 ml):

- 100 units GDH, glucose dehydrogenase
- 20 units diaphorase
- 20  $\mu$ mol NAD
- 30  $\mu$ mol MTT
- 20 25 mg White Saponin
- 1 ml water subjected to ion-exchange

In step 2, the microcuvette was filled with about  
5  $\mu$ l reagent composition solution, the distance between the walls in the sample-absorbing cavity 60, which also  
25 serves as analysing cavity, being about 0.14 mm .

In step 3, the microcuvette was freeze-dried. After  
step 3, the microcuvette contained a dry reagent for  
determination of glucose in undiluted blood uniformly  
distributed in the cavity 60. The microcuvette was then  
30 ready for analysing.

A photometer of the type described above and equipped  
with a microprocessor 18 of the Intel 8751 type was  
provided with a suitable program for determining glucose  
in whole blood. The photometer was programmed in order, at  
35 end-point, to give results on glucose in whole blood  
expressed in mmol/l. The light emitting diodes 38 were



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## CLAIMS

1. Method for determining the glucose content in  
5 whole blood, in which a sample of whole blood is contacted  
with a reagent which by chemical reaction with glucose in  
the sample brings about a dye concentration change which  
is detectable in the sample and the size of which is  
determined as a measure of the glucose content, c h a -  
10 r a c t e r i s e d by the steps of:

introducing the sample undiluted in a microcuvette  
having at least one cavity for receiving the sample, said  
cavity being internally pretreated with the reagent in dry  
form and said chemical reaction then taking place in said  
15 cavity,

selecting as active components included in the rea-  
gent at least a hemolysing agent for exposing glucose  
contained in the blood cells of the sample for allowing a  
quantitative total glucose determination in a whole blood  
20 hemolysate, and agents participating in the chemical reac-  
tion and ensuring that the dye concentration change takes  
place at least in a wavelength range outside the absorp-  
tion range of the blood hemoglobin, and

performing an absorption measurement at said wave-  
25 length range directly on the sample in the cuvette.

2. Method as claimed in claim 1, c h a r a c t e r -  
i s e d in that a glucose dehydrogenase method is used  
for the chemical reaction.

3. Method as claimed in claim 2, c h a r a c t e r -  
30 i s e d in that diaphorase is also selected as active  
component included in the reagent.

4. Method as claimed in any one of claims 1-3,  
c h a r a c t e r i s e d in that mutarotase is also  
selected as active component included in the reagent.

35 5. Method as claimed in any one of claims 1-4,  
c h a r a c t e r i s e d in that, in addition to said  
absorption measurement in said wavelength range in which

said dye concentration change occurs, a secondary absorption measurement is also carried out at a higher wavelength range for providing compensation for background interference.

5           6. Method as claimed in claim 5, c h a r a c t e r -  
i s e d in that the first-mentioned wavelength range, in  
which said dye concentration change occurs, is above  
650 nm and that said secondary wavelength range in which  
said compensation measurement takes place, is above  
10 700 nm, preferably 740-940 nm.

7. Method as claimed in any one of claims 1-6,  
c h a r a c t e r i s e d in that said chemical reaction  
is an end-point reaction, said absorption measurement be-  
ing carried out only when said dye concentration change is  
15 substantially terminated.

8. Disposable cuvette (58) for use in carrying out  
glucose content determination in whole blood where  
a sample of whole blood is contacted with a reagent which  
by chemical reaction with glucose in the sample brings  
20 about a dye concentration change which is detectable in  
the sample and the size of which is determined as a  
measure of the glucose content, c h a r a c t e r -  
i s e d in that the cuvette (58) has at least one cavity  
(60) for receiving the sample, said cavity being internal-  
25 ly pretreated with the reagent in dry form and said chemi-  
cal reaction being intended to take place in said cavity  
after introduction of the sample in undiluted form, that  
active components included in the reagent of the cuvette  
comprise at least one hemolysing agent for exposing  
30 glucose contained in the blood cells of the sample for  
allowing total glucose determination, and agents partici-  
pating in the chemical reaction and ensuring that the dye  
concentration change takes place at least in a wavelength  
range outside the absorption range of the blood  
35 hemoglobin, and that the cuvette is at least partly trans-  
parent for permitting an absorption measurement directly



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on the sample in the cavity of the cuvette in said wavelength range.

9. Photometer for use in carrying out glucose content determination in whole blood where a sample of whole blood is contacted with a reagent which by chemical reaction with glucose in the sample brings about a dye concentration change which is detectable in the sample and the size of which is determined as a measure of the glucose content, c h a r a c t e r i s e d in that the photometer is adapted to be used in combination with an at least partly transparent disposable microcuvette (58) which initially is pretreated with the reagent in dry form and in which the chemical reaction is intended to take place after introduction of the sample in undiluted form in the cuvette, and that the photometer for carrying out an absorption measurement directly on the sample in the cuvette comprises a first light emitting diode (52) having a light wavelength in said wavelength range in which said dye concentration change occurs, a second light emitting diode (64) having a light wavelength separate from said wavelength range, a light detector (40) which during measurement receives light transmitted through the cuvette and the sample, alternately from said first and said second light emitting diode, electronic evaluation means (18, 20, 22, 24; 46) calculating, on the basis of the amount of light measured by the light detector (40), the glucose content of the sample from a difference between the transmittance at the light wavelength of said first light emitting diode (52) and the transmittance at the light wavelength of said second light emitting diode (64), and display means (26, 28) for displaying the glucose content calculated by said evaluation means.

10. Photometer as claimed in claim 9, c h a r a c t e r i s e d in that the light wavelength of said first light emitting diode (52) is above 650 nm and that the

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light wavelength of said second light emitting diode (64) is above 700 nm.

11. Photometer as claimed in claim 9 or 10, characterised in that the light from at least one (58) of said light emitting diodes is caused to pass through a monochromatic filter (54).

12. Photometer as claimed in claim 10, characterised in that the light wavelength of the second light emitting diode (64) is within the range of 740-940 nm.

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Fig.1

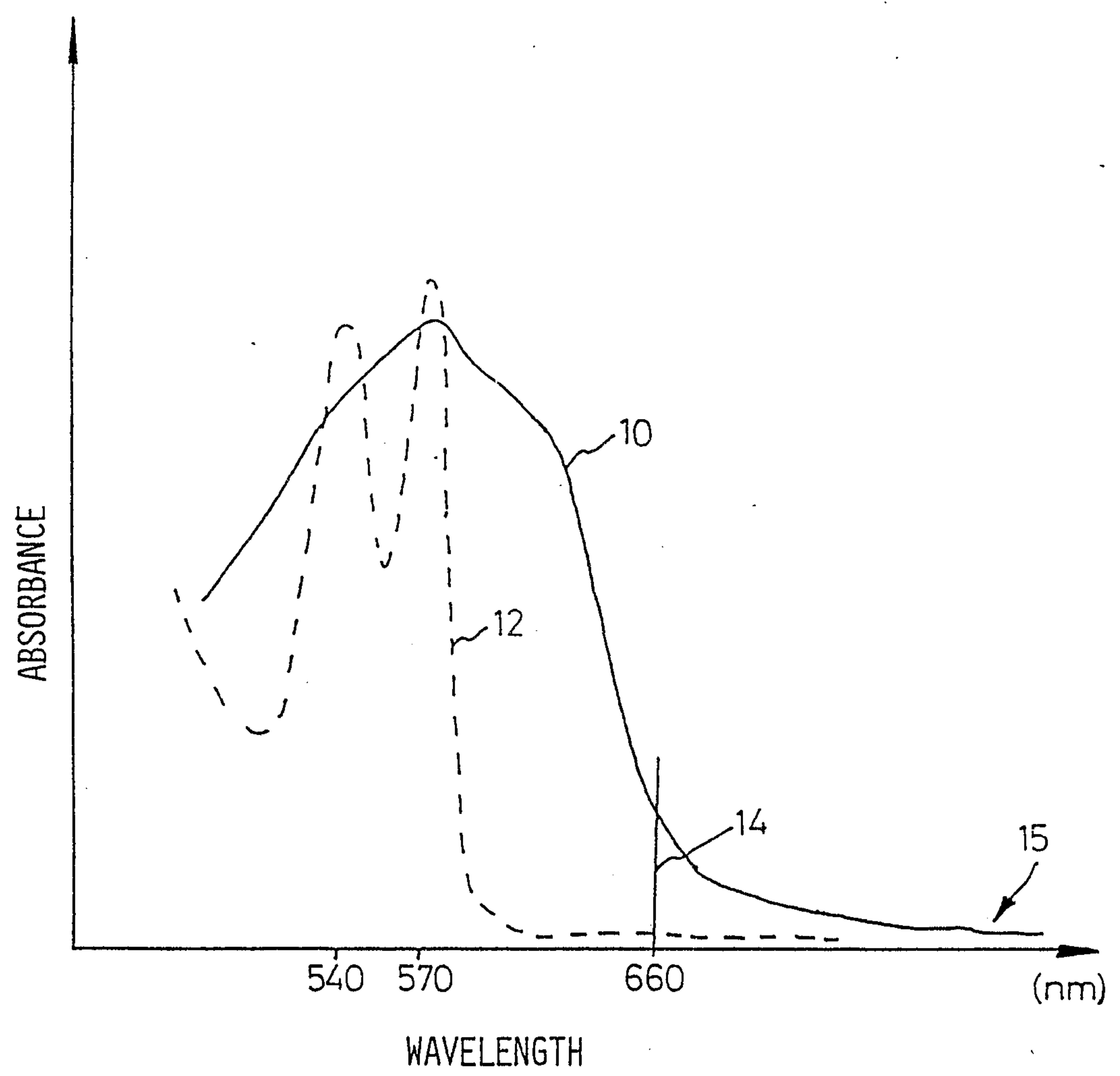
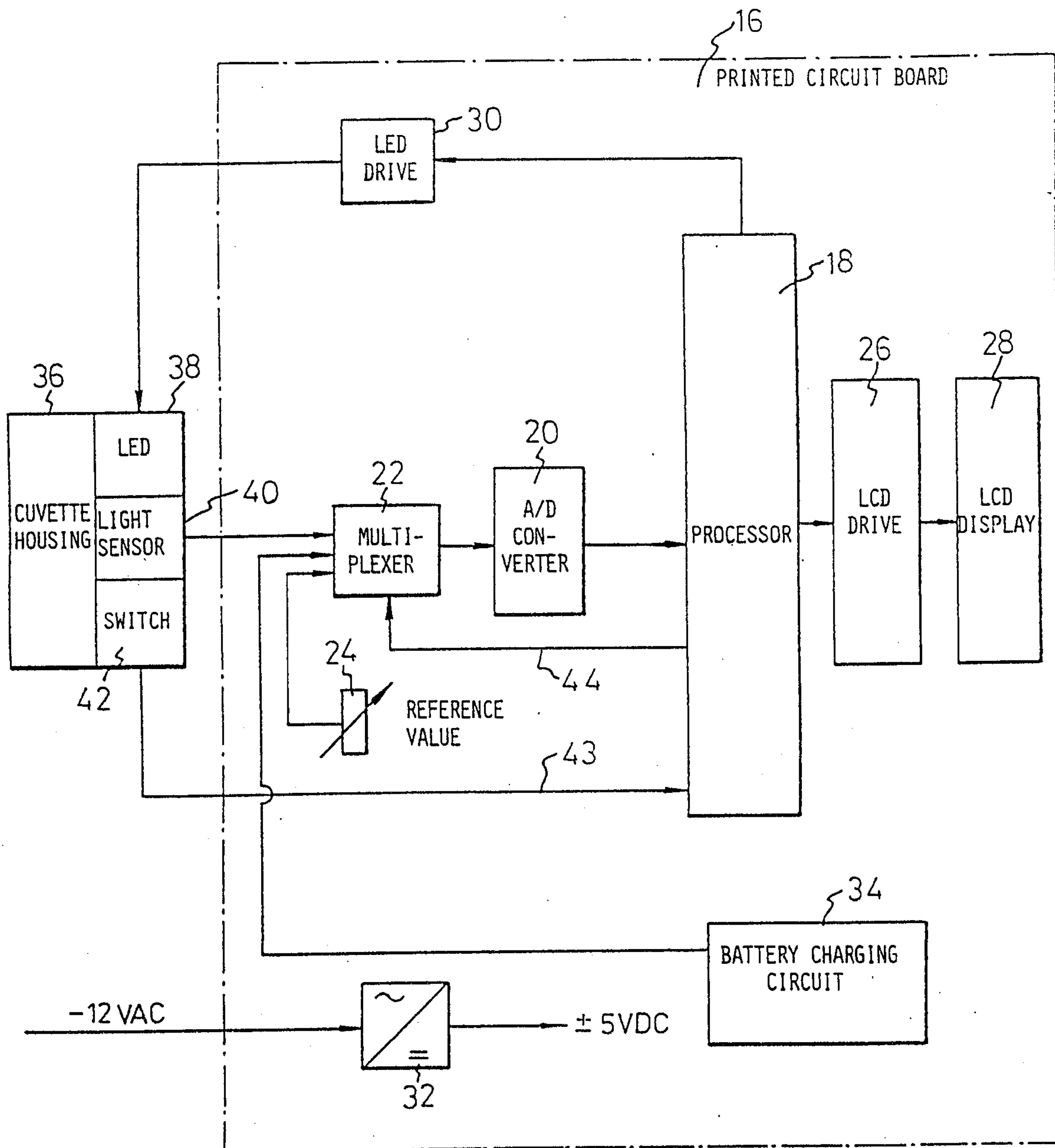


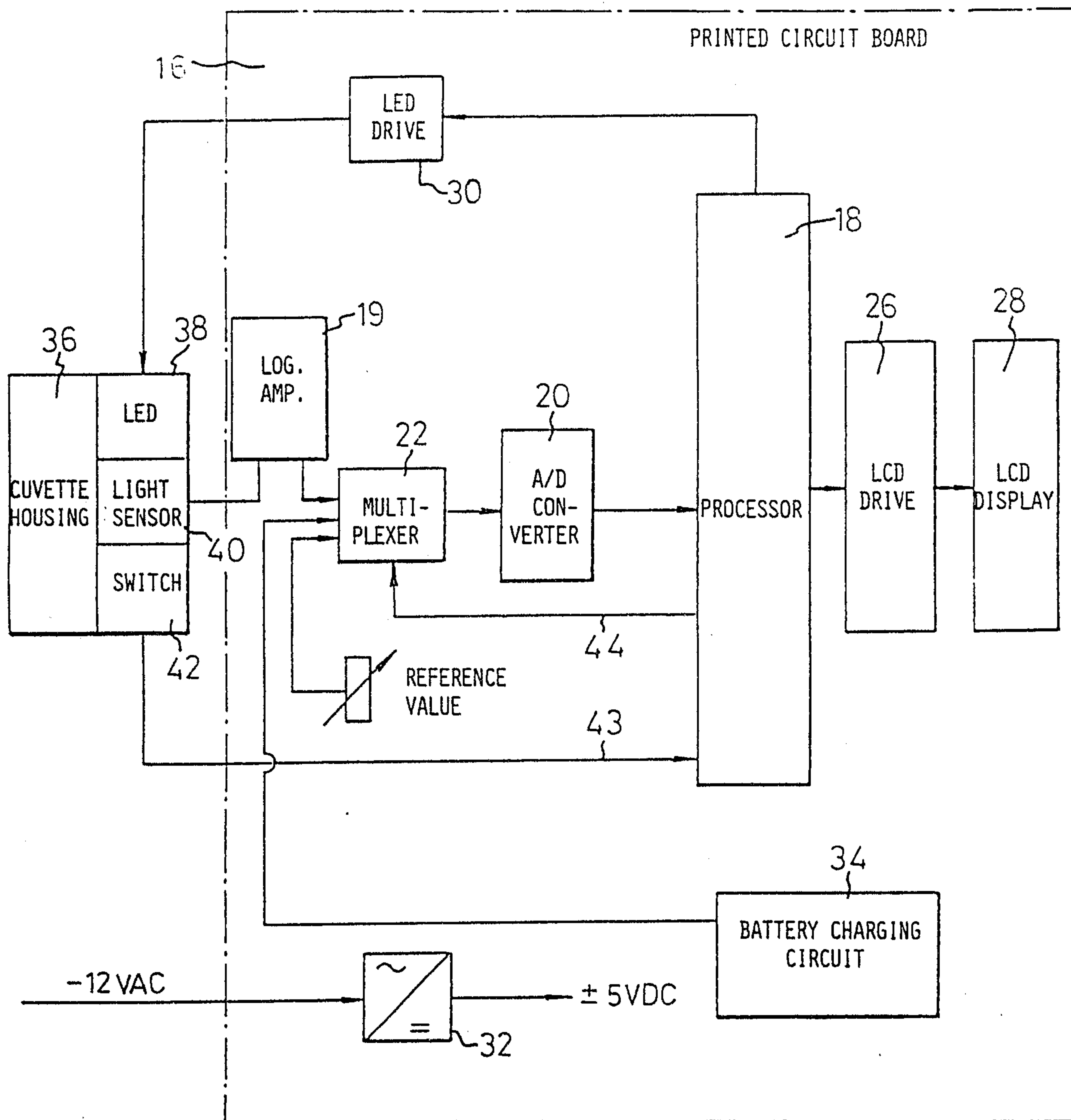
Fig. 2A





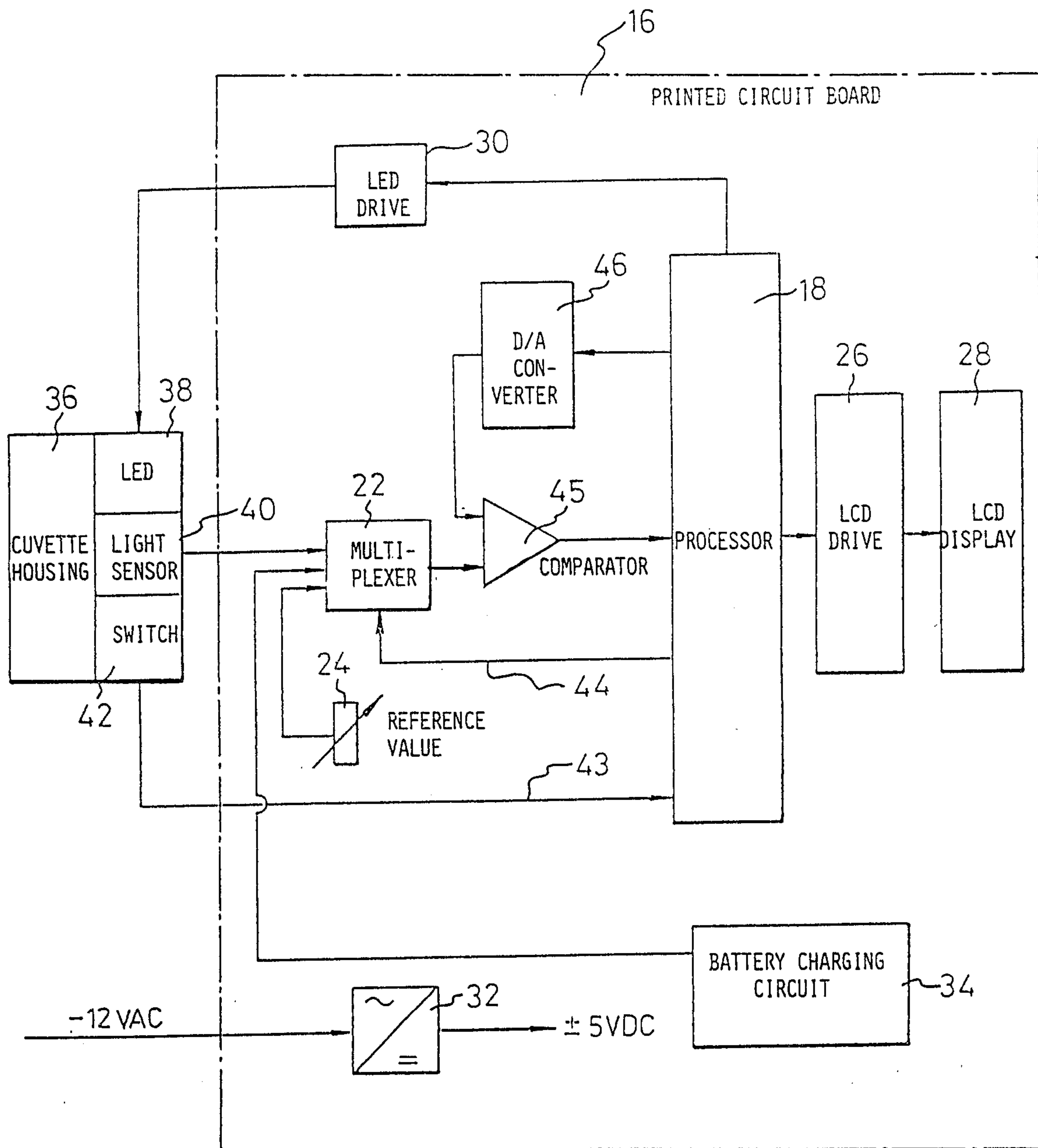
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Fig. 2 B



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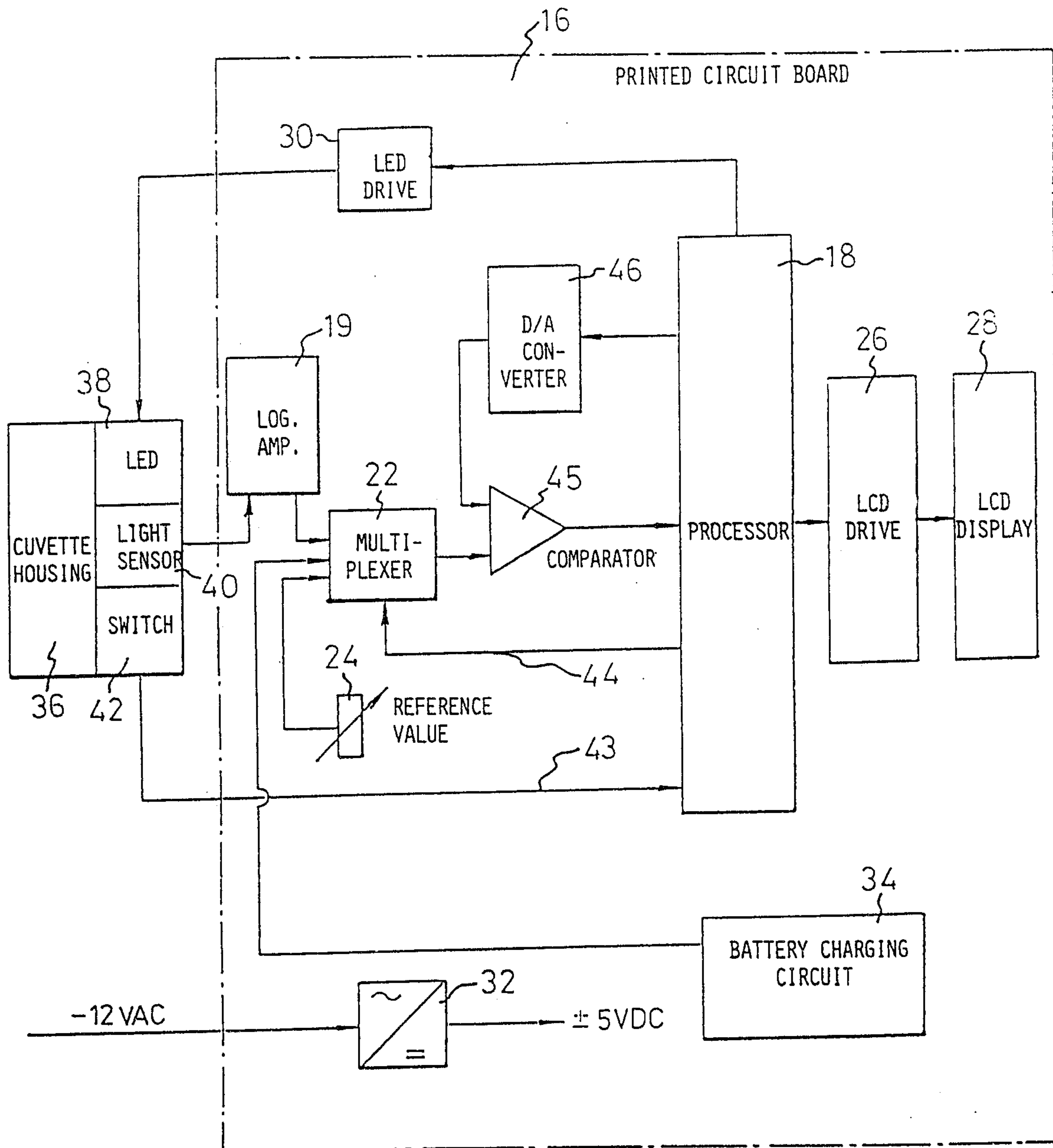
Fig. 3A





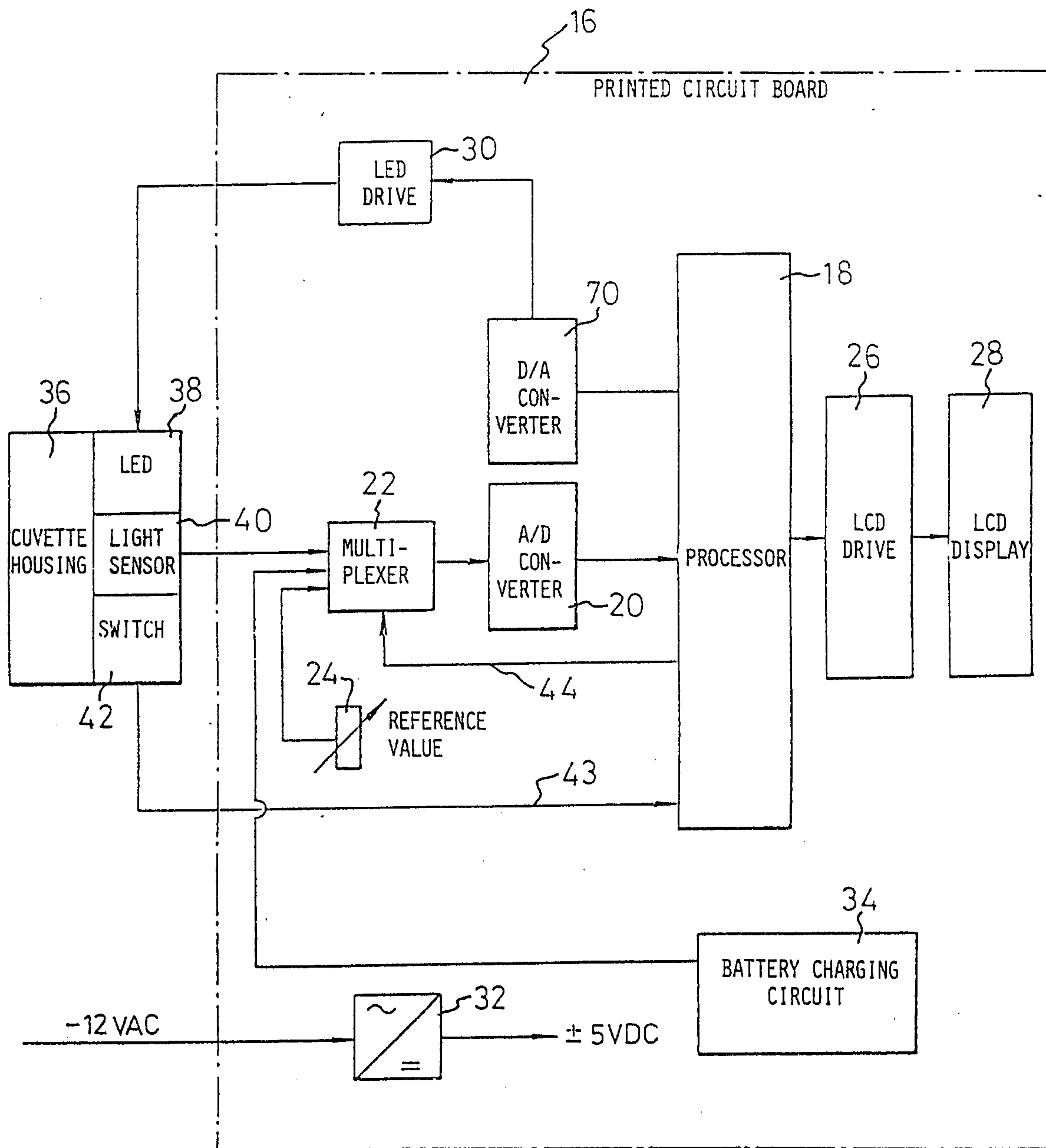
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Fig.3 B



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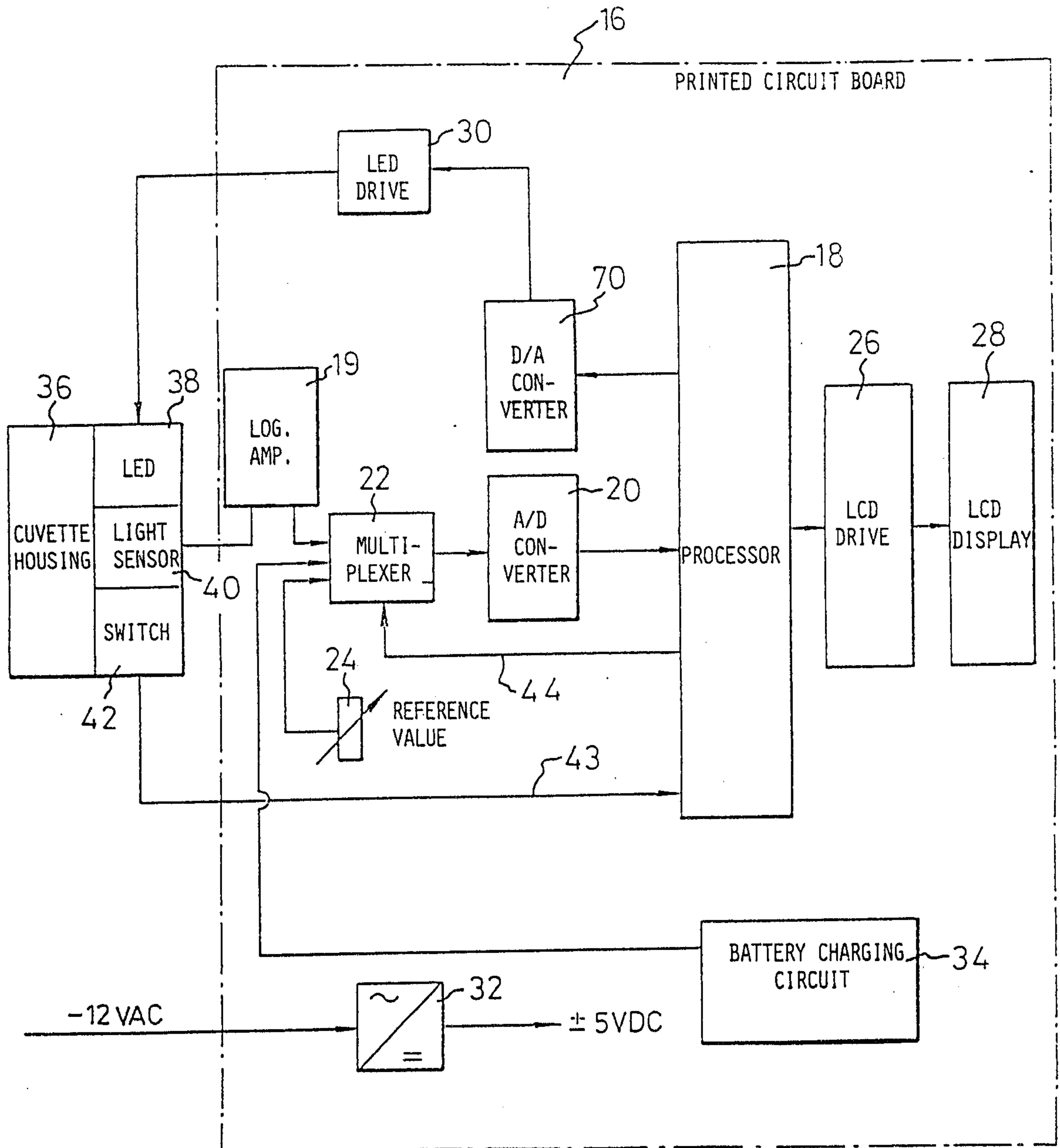
Fig.4 A





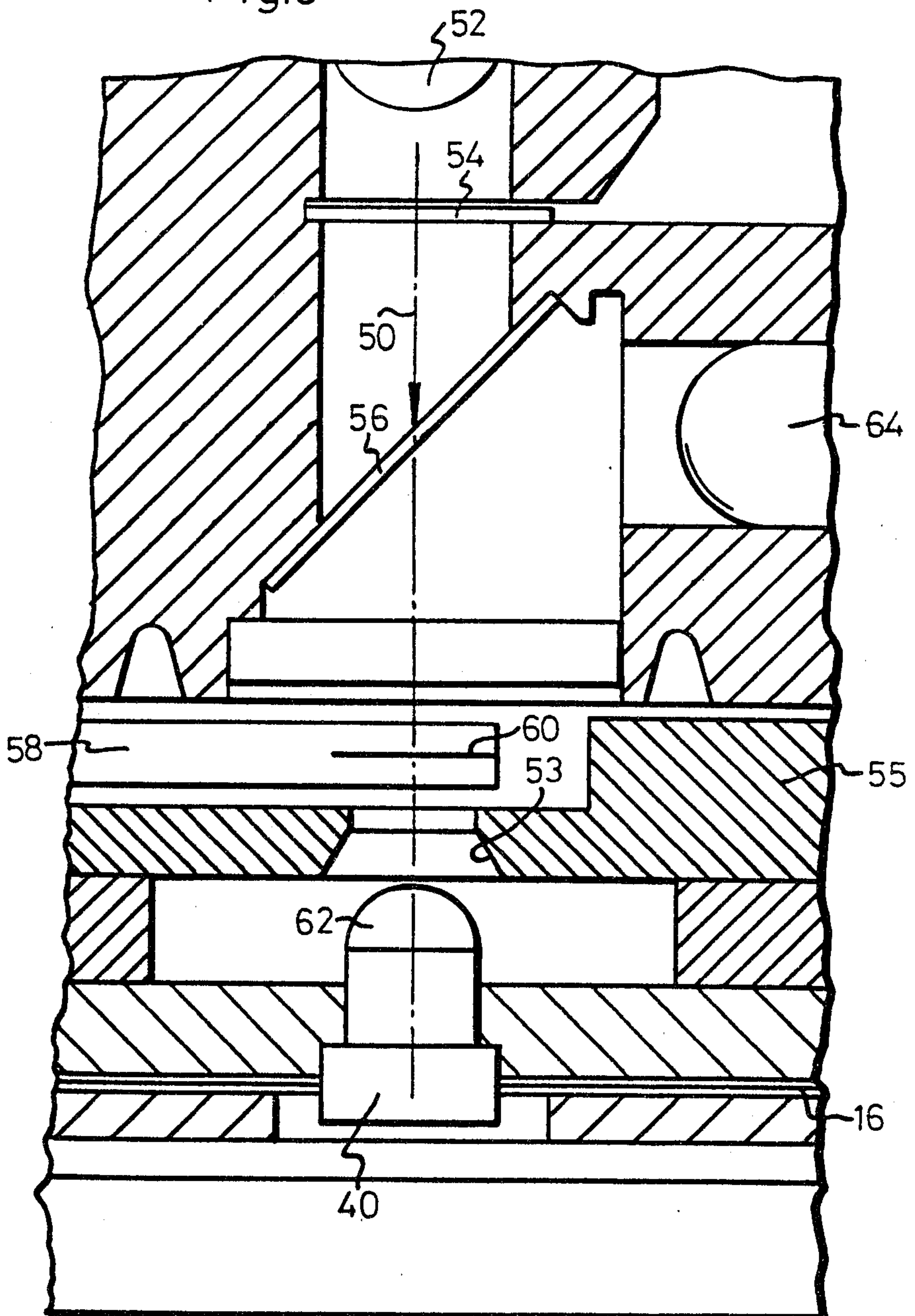
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Fig. 4 B



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Fig.5



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