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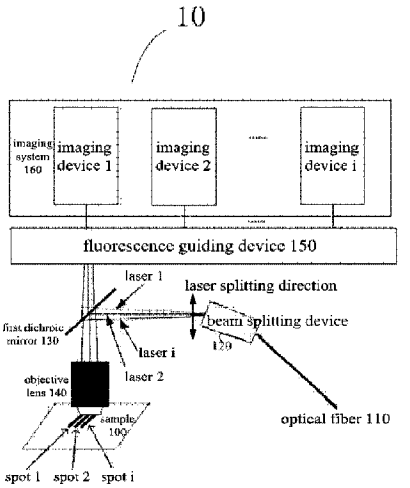


FIG. 1a

(57) Abrégé/Abstract:
The present invention provides a detection device, a system, and a method, and belongs to the technical field of detection. The detection device comprises a beam splitting apparatus, a first dichroscope, an objective lens, a fluorescence guide apparatus, and an imaging system comprising a plurality of imaging apparatuses. The beam splitting apparatus receives and separates incident laser that has a plurality of different wavelengths and comes from an optical fiber. The first dichroscope receives a plurality of excitation lasers emitted from the beam splitting apparatus and transmits the plurality of excitation lasers to the objective lens, as well as receives a plurality of fluorescence and transmits the fluorescence to the fluorescence guide apparatus. The objective lens receives the excitation lasers, respectively focuses the excitation lasers on a plurality of different regions of a sample so as to excite fluorescence, and transmits a plurality of fluorescence to the first dichroscope. The fluorescence guide apparatus receives the plurality of fluorescence transmitted by the first dichroscope and respectively guides the plurality of fluorescence to the imaging apparatuses. In the present invention, the power density of a laser on a sample can be reduced in the scenario in which the detection duration is not increased, and the problem in the existing technology that the aspects of "high speed" and "high detection quality and long read length" are not compatible is solved.

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ABSTRACT

The present disclosure provides a detecting apparatus, system, and method, and belongs to the technical field of detection. The detecting apparatus includes a beam splitting device, a first dichroic mirror, an objective lens, a fluorescence guiding device, and an imaging system including a plurality of imaging devices. The beam splitting device receives and separates an incident light beam of a plurality of different wavelengths that is formed by lasers from the optical fiber, and to form a plurality of excitation lasers corresponding to the plurality of different wavelengths of the incident light beam; the first dichroic mirror receives the plurality of excitation lasers exiting from the beam splitting device and transmits them to the objective lens, and receives a plurality of fluorescence and transmits them to the fluorescence guiding device; the objective lens receives the plurality of excitation lasers and focuses them respectively on a plurality of different areas of a sample to excite fluorescence, and transmits the plurality of fluorescence to the first dichroic mirror; and the fluorescence guiding device receives the plurality of fluorescence transmitted via the first dichroic mirror and guides the plurality of fluorescence to the plurality of imaging devices respectively. The present disclosure makes it possible to reduce the power density of the laser on the sample without increasing the detection duration, solving the problem that the two aspects of "high speed" and "high detection quality and long read length" cannot be better compatible in the related arts.

DETECTING APPARATUS, GENE SEQUENCING SYSTEM, AND DETECTING METHOD

FIELD

[0001] The present disclosure relates to the technical field of detection, and more particularly, to a detecting apparatus, a gene sequencing system, and a detecting method.

BACKGROUND

[0002] In the field of biochemical detection, it is known to irradiate a sample with a laser to excite the sample to generate fluorescence and detect the generated fluorescence so as to achieve desired detection of the sample. Some related arts will be introduced below by taking gene detection as an example.

[0003] The gene detection is completed by exciting a sample by a laser to generate fluorescence, and then detecting and analyzing the generated fluorescence by using an imaging system to obtain a target base sequence. A variety of bases existing on a sample to be detected are labeled by different primers to trace, with the primers being excited by lasers of different wavelengths to obtain corresponding fluorescence (corresponding to the bases in a one-to-one correspondence). In the process of fluorescence excitation, there are accompanying phenomena of photobleaching and fluorescence crosstalk, of which the phenomenon of photobleaching greatly reduces the fluorescence yield and even denaturalizes the fluorescence, resulting in deterioration of the detection result, and the phenomenon of fluorescence crosstalk refers to the following phenomenon: some primers, when being excited to obtain excited fluorescence, are influenced by the excitation process of other primers, causing the quantum yield to be influenced, and multiple fluorescence is generated simultaneously in an area and mixed with each other. The higher the power density of excitation light, the longer the excitation duration and the longer

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the detection read length, the more obvious the phenomena of photobleaching and fluorescence crosstalk.

[0004] In order to pursue high speed, high throughput, and low cost, the laser power density used in the detecting system is getting higher and higher, and the accompanying phenomenon of photobleaching and phenomenon of fluorescence crosstalk seriously affect the sequencing quality and restrict the base sequence length (read length) detectable by the gene detection. In particular, the new generation of high-speed and high-throughput gene detection technology adopts a Time Delay Integration (TDI) imaging technology, which uses the method of lasers of multiple wavelengths simultaneously exciting fluorescence and performing high-speed scanning, and the laser power density used is hundreds of times higher than that adopted in a conventional area array imaging method. With the increase in the detection read length, the influence of the laser of high power density becomes more and more obvious, which leads to the detection quality decreasing faster and faster. The related gene detection technology cannot be better compatible with both "high speed" and "high detection quality and long read length".

[0005] In order to reduce the illumination cost and the structural complexity, the existing gene detecting apparatus coaxially outputs lasers of different wavelengths through an optical fiber. When passing through a beam shaping device and an objective lens, main light beams of all wavelengths are coaxially transmitted and finally irradiate on a same area of the sample. At this time, there are two choices, simultaneous excitation and time-division excitation.

[0006] FIG. 6 shows a known apparatus 60 for implementing a first related art (i.e. simultaneous excitation). As shown in FIG. 6, when the first related art (i.e., simultaneous excitation) is adopted, a multimode optical fiber 610 outputs n lasers of different wavelengths simultaneously (n is the number of lasers of different wavelengths, the same below), the lasers are shaped by a beam shaping device 670, filtered by a laser filter 620, reflected by a first dichroic mirror 630, focused by an objective lens 640, etc., and then focused on a sample 600, and the n lasers of different wavelengths are focused on a same position (a position where a spot formed by the lasers of multiple wavelengths in FIG. 6 is) of the sample and excite fluorescence at the position on the sample. Then, the fluorescence is detected by the objective lens 640, then is transmitted through the first dichroic mirror 630, and then passes through further specific

dichroic mirrors (i.e., dichroic mirror 1, dichroic mirror 2, ... dichroic mirror n) constituting a fluorescence guiding device 650, and then through specific optical filters (i.e., optical filter 1, optical filter 2, ... optical filter n; each optical filter may only transmit fluorescence of a specific wavelength), so that the fluorescence of different wavelengths is split, and then the fluorescence of different wavelengths passes through imaging lenses (i.e., imaging lens 1, imaging lens 2,... imaging lens n) corresponding to the fluorescence of different wavelengths in an imaging system 660, and then is photographed by cameras (i.e., camera 1, camera 2,... camera n) corresponding to the imaging lenses in the imaging system 660 to output fluorescence information, with the fluorescence excited by the nth laser being transmitted through the nth optical filter corresponding thereto, being focused by the imaging lens n and then being received by the camera n. In this way, the process of simultaneous excitation, and simultaneous detection, of fluorescence can be completed. The detection speed of fluorescence of each Field of View (FOV) is equal to the time for single shot of the camera, and the laser power in the illumination area is the sum of the power of all lasers, that is, the density becomes n times that in the case of irradiation by a single laser (assuming that the laser power density of each wavelength is the same). At a high power density, the fluorescence is more severely influenced by photobleaching, and the phenomenon of fluorescence crosstalk exists among different channels, which both affect the accuracy of detection results. To conclude, the first related art focuses on "high speed", and the method thereof is as follows: the fluorescence is excited by n lasers of different wavelengths simultaneously, the fluorescence detection of all channels can be completed by only one shot in an area of a single FOV, but the power density is n times of that in the case of irradiation by a laser of a single wavelength.

[0007] FIG. 7 shows a known apparatus 70 for implementing a second related art (i.e. time-division excitation). As shown in FIG. 7, when the second related art (i.e., time-division excitation) is adopted, a multimode optical fiber 710 sequentially outputs n lasers of different wavelengths, and the output lasers are focused at a position (i.e., the position where a spot of laser at different time in FIG. 7 is) of a sample 700 after being shaped by a beam shaping device 770, filtered by a laser filter 720, reflected by a dichroic mirror 730, and focused by an objective lens 740, etc., and excite fluorescence at the position on the sample. The fluorescence is detected

by the objective lens 740, then is transmitted through the dichroic mirror 730, a fluorescence filter 750 (which only transmits the fluorescence and filters out stray light other than the fluorescence), and an imaging lens 760, and then is photographed by a camera 780 to output fluorescence information. Only by n shots, can the fluorescence detection of the FOV be completed. All the lasers need to be output by the multimode optical fiber in sequence and the fluorescence detection is performed in sequence accordingly; that is, the power density of the laser irradiating on the sample is the same as that in the case of irradiation by a single laser (assuming that the power density of each laser is the same). Therefore, the phenomenon of photobleaching is relatively weak and the crosstalk between fluorescence is reduced. However, the fluorescence detection time for each FOV is increased to n times that for a single shot. To conclude, the second related art focuses on "high detection quality and long read length" and the method thereof is as follows: n lasers of different wavelengths excite the fluorescence in turn sequentially (at the same time, cameras corresponding thereto in a one-to-one correspondence take images for fluorescence detection), the power density is the same as that when a single laser excites the fluorescence, but n times of excitation and n times of fluorescence detection are required, the total duration of the fluorescence detection is n times that for the first related art, and the total detection time required for detecting a same sample is n times that for the first related art.

[0008] Although the first related art improves the detection speed, the power density of the laser irradiation is increased by n times, different fluorescence is excited at the same position, the phenomenon of photobleaching is obvious, and there is the fluorescence crosstalk, resulting in the decrease of the fluorescence yield. With the increase of the read length, the second related art is obviously superior to the first related art in the detection error rate, but has the shot time become n times as compared with the first related art.

[0009] Therefore, an improved solution for biochemical detection is needed to solve or alleviate the problems of photobleaching and fluorescence crosstalk caused by the high optical power density, while giving due consideration to the detection speed.

SUMMARY

[0010] The purpose of the present disclosure is to provide an improved solution for biochemical detection, to solve or mitigate the problems of photobleaching and fluorescence crosstalk caused by high optical power density while giving due consideration to the detection speed.

[0011] According to a first aspect of the present disclosure, a detecting apparatus is provided, the detecting apparatus comprising a beam splitting device, a first dichroic mirror, an objective lens, a fluorescence guiding device, and an imaging system including a plurality of imaging devices, wherein,

[0012] the beam splitting device is configured to receive and separate an incident light beam of a plurality of different wavelengths from an optical fiber, to form a plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam emitted in different emitting directions from the beam splitting device, wherein, each of the excitation light beams has a wavelength in a one-to-one correspondence with the plurality of different wavelengths of the incident light beam;

[0013] the first dichroic mirror is positioned to receive the plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam in a one-to-one correspondence and emitted from the beam splitting device, to transmit the plurality of excitation light beams to the objective lens, such that the plurality of excitation light beams are focused respectively on a plurality of different areas of a sample to be detected through the objective lens, to excite a plurality of fluorescence in the plurality of different areas of the sample on which the plurality of excitation light beams are focused respectively, and to receive the plurality of fluorescence excited by the plurality of excitation light beams respectively and transmit the plurality of fluorescence to the fluorescence guiding device;

[0014] the objective lens is positioned to receive the plurality of excitation light beams transmitted by the first dichroic mirror, to focus the plurality of excitation light beams on the plurality of different areas of the sample respectively, and to transmit the plurality of fluorescence excited by the plurality of excitation light beams respectively to the first dichroic mirror;

[0015] the fluorescence guiding device is positioned to receive the plurality of fluorescence transmitted by the first dichroic mirror, and to guide the plurality of fluorescence to the plurality of imaging devices respectively, such that each fluorescence of the plurality of fluorescence is imaged by one of the plurality of imaging devices corresponding to the fluorescence; and

[0016] each of the plurality of imaging devices is positioned to receive one fluorescence of the plurality of fluorescence guided by the fluorescence guiding device, and to image the fluorescence to obtain fluorescence information corresponding to the fluorescence for detection.

[0017] According to a second aspect of the present disclosure, a gene sequencing system is provided, the gene sequencing system comprising an imaging system for collecting a fluorescence signal on a sequencing chip; and an optical system located between the imaging system and the sequencing chip, characterized in that the optical system comprises:

[0018] a light source configured to emit an incident light beam of a plurality of different wavelengths;

[0019] a beam splitting device configured to receive and separate the incident light beam of a plurality different wavelengths from the light source, to form a plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam emitted in different emitting directions from the beam splitting device, wherein, each of the excitation light beams has a wavelength in a one-to-one correspondence with the plurality of different wavelengths of the incident light beam;

[0020] a first dichroic mirror configured to receive the plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam in a one-to-one correspondence and emitted from the beam splitting device;

[0021] an objective lens arranged between the sequencing chip and the first dichroic mirror and configured to receive the plurality of excitation light beams transmitted by the first dichroic mirror, to focus the plurality of excitation light beams on a plurality of different areas on the sequencing chip to excite a plurality of fluorescence in the plurality of different areas in one-to-one correspondence with the plurality of excitation light beams respectively, and to transmit the plurality of fluorescence to the first dichroic mirror; and

[0022] a fluorescence guiding device configured to receive the plurality of fluorescence

transmitted via the first dichroic mirror and to guide the plurality of fluorescence to the imaging system respectively,

[0023] wherein the imaging system comprises a plurality of imaging devices corresponding to the plurality of fluorescence in a one-to-one correspondence, each of the plurality of imaging devices being configured to receive one fluorescence, which corresponds to the imaging device, of the plurality of fluorescence guided by the fluorescence guiding device, and to image the fluorescence to obtain fluorescence information corresponding to the fluorescence.

[0024] According to a third aspect of the present disclosure, a detecting method is provided, the detecting method comprising:

[0025] emitting, by a light source or a light conduction device, an incident light beam of a plurality of different wavelengths;

[0026] receiving and separating, by a beam splitting device, the incident light beam of a plurality of different wavelengths from the light source or the light conduction device, to form a plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam emitted in different emitting directions from the beam splitting device, wherein, each of the excitation light beams has a wavelength in a one-to-one correspondence with the plurality of different wavelengths of the incident light beam;

[0027] receiving, by a first dichroic mirror, the plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam in a one-to-one correspondence and emitted from the beam splitting device;

[0028] receiving, by an objective lens arranged between a sample to be detected and the first dichroic mirror, the plurality of excitation light beams transmitted by the first dichroic mirror, focusing, by the objective lens, the plurality of excitation light beams on a plurality of different areas on the sample to excite a plurality of fluorescence in the plurality of different areas in one-to-one correspondence with the plurality of excitation light beams respectively, and transmitting, by the objective lens, the plurality of fluorescence to the first dichroic mirror; and

[0029] receiving, by a fluorescence guiding device, the plurality of fluorescence transmitted by the first dichroic mirror, and guiding, by the fluorescence guiding device, the plurality of fluorescence to a plurality of imaging devices corresponding to the plurality of fluorescence in

a one-to-one correspondence, such that each fluorescence of the plurality of fluorescence is received and imaged by one of the plurality of imaging devices corresponding to the fluorescence to obtain fluorescence information corresponding to the fluorescence for detection.

[0030] Through an inventive configuration, the present disclosure enables light of different wavelengths to simultaneously and separately illuminate different positions on the sample to be detected, so as to simultaneously excite the fluorescence at the different positions. Taking a laser used as excitation light as an example, the power density of the laser on the sample is reduced to 1/n of the laser density in the case of simultaneous excitation, and the fluorescence detection of all channels can be completed by only a single excitation in an area of a single field of view, and the total detection time is equal to the time required for a single fluorescence excitation and detection when the fluorescence is excited multiple times in a same area for detection (i.e., in the case of time-division excitation). By using the solution of the present disclosure, the power density of the laser on the sample can be reduced without increasing the detection duration, solving the problem that the two aspects of "high speed" and "high detection quality and long read length" cannot be better compatible in the related arts; that is, the problem of photobleaching and fluorescence crosstalk caused by high optical power density can be solved or alleviated, while due consideration can be given to the detection speed.

BRIEF DESCRIPTION OF THE DRAWINGS

[0031] FIG. 1a is a schematic diagram of the composition and structure of a detecting apparatus according to an exemplary embodiment of the present disclosure;

[0032] FIG. 1b is a schematic diagram of the composition and structure of an exemplary fluorescence guiding device that can be used in a detecting apparatus of the present disclosure;

[0033] FIG. 1c is a schematic diagram of the composition and structure of another exemplary fluorescence guiding device that can be used in a detecting apparatus of the present disclosure;

[0034] FIG. 2 is a schematic diagram of the composition and structure of a detecting apparatus according to another exemplary embodiment of the present disclosure;

[0035] FIG. 3 is a schematic diagram showing a detecting apparatus according to yet another exemplary embodiment of the present disclosure;

[0036] FIG. 4 is a schematic diagram schematically showing spots formed on a surface of a sample by two excitation lasers when detection is performed using a detecting apparatus according to an exemplary embodiment of the present disclosure;

[0037] FIG. 5 is a schematic diagram schematically showing a process of performing fluorescence integration scanning in an exemplary embodiment using a TDI imaging technology;

[0038] FIG. 6 schematically shows a known apparatus for implementing a related detection technology adopting simultaneous excitation;

[0039] FIG. 7 schematically shows a known apparatus for implementing a related detection technology adopting time-division excitation;

[0040] FIG. 8a shows a relation between a data quality Q30 and a read length for gene detection results obtained by performing a double-end test on DNA sequences under the same conditions, using a related technology adopting simultaneous excitation, using a related technology adopting time-division excitation, and using the present disclosure; and

[0041] FIG. 8b shows a relation between a detection error rate and a read length for gene detection results obtained by performing a double-end test on DNA sequences under the same conditions, using a related technology adopting simultaneous excitation, using a related technology adopting time-division excitation, and using the present disclosure.

DETAILED DESCRIPTION

[0042] The exemplary embodiments of the present disclosure will be described in detail with reference to the accompanying drawings, which form a part of the present disclosure, and which, together with the embodiments of the present disclosure, serve to explain the principle of the present disclosure. For the purpose of clarity and simplification, a detailed specific description of the known functions and structures of the devices described herein will be omitted when it may obscure the subject matter of the present disclosure.

[0043] A detecting apparatus 10 according to an exemplary embodiment of the present

disclosure, as shown in FIG. 1, includes the following components: a beam splitting device 120, a first dichroic mirror 130, an objective lens 140, a fluorescence guiding device 150, and an imaging system 160 including imaging device 1 to imaging device i, where i represents a number of different wavelengths of incident laser(s) from an optical fiber and is an integer greater than 1.

[0044] The beam splitting device 120 is configured to receive and separate the incident laser(s) of a plurality of different wavelengths from the optical fiber, such that when the incident laser(s) of the plurality of different wavelengths is/are emitted in different emitting direction(s) from the beam splitting device, each excitation laser corresponding thereto, such as laser 1, laser 2, and laser i shown in FIG. 1, is formed. The wavelength of each excitation laser is the same as the wavelength of the incident laser corresponding to the excitation laser. The beam splitting device may be implemented by various optical devices having a dispersive capability or a combination of such optical devices. For example, the beam splitting device may be, for example, a single dispersion prism, a plurality of dispersion prisms, one or more gratings, and the like, as will be further described later, depending on the specific situation of the actual application and the corresponding requirements. The optical fiber may be a single optical fiber, for example but not limited to a coupled optical fiber. It is advantageous, although not essential, that the incident laser(s) of a plurality of different wavelengths may be incident on the beam splitting device in the same incident direction. Although the incident laser(s) is/are transmitted to the beam splitting device by the optical fiber in FIG. 1, it is possible to provide the incident laser(s) to the beam splitting device with another optical transmission device instead of the optical fiber. The optical fiber or the another optical transmission device may be included in or outside the detecting apparatus.

[0045] The first dichroic mirror 130 is positioned to receive the plurality of excitation lasers corresponding to the incident laser(s) of a plurality of different wavelengths respectively and emitted from the beam splitting device, to transmit the excitation laser(s) to the objective lens in such a manner that the plurality of excitation lasers are respectively focused on a plurality of different areas of a sample to be detected 100 (such as positions where spot 1, spot 2, and spot i in FIG. 1 are located) through the objective lens to excite fluorescence in the corresponding

areas of the sample on which they are focused respectively, and to receive a plurality of fluorescence that are excited by the plurality of excitation lasers respectively and transmit the plurality of fluorescence to the fluorescence guiding device. In FIG. 1, the focusing spots of laser 1, laser 2, and laser i on the sample are schematically shown by spot 1, spot 2, and spot i. Here, the sample to be detected may be various substances that can emit fluorescence when irradiated by a laser, for example but being not limited to, a biological sample, a chemical sample, and the like. The first dichroic mirror may be suitably oriented in such a manner that the plurality of excitation lasers corresponding to the incident laser(s) of a plurality of different wavelengths respectively and emitted from the beam splitting device are all received by the first dichroic mirror, and after being reflected by the first dichroic mirror, are all focused by the objective lens on the plurality of different areas of the sample, and the plurality of fluorescence that is excited by the plurality of excitation lasers respectively and received from the sample via the objective lens is all transmitted to the fluorescence guiding device via the first dichroic mirror. On this premise, the orientation of the first dichroic mirror may be determined, for example, based on the exit angle of each excitation laser relative to the beam splitting device and the objective lens. Depending on the situation, the first dichroic mirror may be placed at different angles.

[0046] The objective lens 140 is positioned to receive the plurality of excitation lasers transmitted via the first dichroic mirror, to focus the plurality of excitation lasers on the plurality of different areas of the sample respectively, and to transmit the plurality of fluorescence excited by the plurality of excitation lasers respectively to the first dichroic mirror. Generally, the objective lens is a lens group composed of a single lens or a combination of multiple lenses. The lens(es) may include, for example, but is not limited to, a convex lens, a concave lens, a glued lens, and the like.

[0047] The fluorescence guiding device 150 is positioned to receive the plurality of fluorescence transmitted via the first dichroic mirror and to guide the plurality of fluorescence to the plurality of imaging devices respectively, such that each fluorescence of the plurality of fluorescence is imaged by one of the plurality of imaging devices corresponding to the fluorescence. The fluorescence guiding device may be implemented in various possible ways. For example, the fluorescence guiding device may be a plurality of second dichroic mirrors

provided as required and the number of the plurality of second dichroic mirrors may be equal to the number of the excitation lasers, i.e., i. At this time, depending on the situation, each second dichroic mirror may be arranged to achieve one of: transmitting a certain fluorescence and reflecting the remaining fluorescence, and reflecting a certain fluorescence and transmitting the remaining fluorescence, such that the combination of the plurality of second dichroic mirrors achieves the desired guidance of the fluorescence as described above. Each of the plurality of fluorescence guided by the fluorescence guiding device corresponds to each of the plurality of imaging devices in a one-to-one correspondence. According to one possible implementation, the fluorescence guiding device includes a plurality of second dichroic mirrors that are sequentially arranged, the plurality of second dichroic mirrors including a last second dichroic mirror that is away from the first dichroic mirror and at least one preceding second dichroic mirror located between the last second dichroic mirror and the first dichroic mirror, the plurality of fluorescence received by the first dichroic mirror propagating sequentially through the plurality of second dichroic mirrors, each of the preceding second dichroic mirror(s) is positioned to guide one of at least one fluorescence incident thereon among the plurality of fluorescence to a corresponding imaging device, and to guide remaining fluorescence of the at least one fluorescence to a next second dichroic mirror adjacent thereto, and the last second dichroic mirror is positioned to guide fluorescence incident thereon to a corresponding imaging device.

[0048] Specifically, for example, referring to an exemplary fluorescence guiding device 150' shown in FIG. 1b, the fluorescence guiding device 150' includes a plurality of second dichroic mirrors that are sequentially arranged: dichroic mirror 1, dichroic mirrors 2, ..., dichroic mirror i. The second dichroic mirror located closest to the first dichroic mirror of the at least one preceding second dichroic mirror among the plurality of second dichroic mirrors, i.e., the dichroic mirror 1, can be selected to transmit the fluorescence that is guided by it to the corresponding imaging device among the plurality of fluorescence from the first dichroic mirror and reflect the remaining fluorescence of the plurality of fluorescence incident thereon to a next second dichroic mirror that is adjacent to it, i.e., the dichroic mirror 2, the last second dichroic mirror of the plurality of second dichroic mirrors, i.e., the dichroic mirror i, is selected to guide the fluorescence incident thereon to the corresponding imaging device through reflection, and

for each of the second dichroic mirror(s) in the plurality of second dichroic mirrors other than the second dichroic mirror located closest to the first dichroic mirror and the last second dichroic mirror, for example, the dichroic mirror 2, it is selected to reflect the fluorescence that is guided by it to the corresponding imaging device and transmit the remaining fluorescence of the at least one fluorescence incident thereon to a next second dichroic mirror that is adjacent to it.

[0049] As another example, referring to an exemplary fluorescence guiding device 150" shown in FIG. 1c, the fluorescence guiding device 150" includes a plurality of second dichroic mirrors that are sequentially arranged: dichroic mirror 1, dichroic mirror 2, ..., dichroic mirror i. The second dichroic mirror located closest to the first dichroic mirror of the at least one preceding second dichroic mirror among the plurality of second dichroic mirrors, i.e., the dichroic mirror 1, is selected to reflect the fluorescence that is guided by it to the corresponding imaging device among the plurality of fluorescence from the first dichroic mirror and transmit the remaining fluorescence of the plurality of fluorescence incident thereon to a next second dichroic mirror that is adjacent to it, i.e., the dichroic mirror 2, the last second dichroic mirror of the plurality of second dichroic mirrors, i.e., the dichroic mirror i, is selected to guide the fluorescence incident thereon to the corresponding imaging device through reflection, and for each of the second dichroic mirror(s) in the plurality of second dichroic mirrors other than the second dichroic mirror located closest to the first dichroic mirror and the last second dichroic mirror, for example, the dichroic mirror 2, it is selected to reflect the fluorescence that is guided by it to the corresponding imaging device and transmit the remaining fluorescence of the at least one fluorescence incident thereon to a next second dichroic mirror that is adjacent to it.

[0050] A dichroic mirror may be positioned in such a manner that light to be received by it is incident thereon at an incident angle in a certain range, which facilitates reflection and/or transmission of the received light by the dichroic mirror, especially in the case of mixed light. The positioning of the dichroic mirror may be determined by considering an upstream component that transmits light to the dichroic mirror. The range may be, for example, an angular range including 45 degrees. Different dichroic mirrors can have different incident angle ranges required by design.

[0051] Each of the plurality of imaging devices is positioned to receive a fluorescence

corresponding thereto of the plurality of fluorescence guided by the fluorescence guiding device, and to image the fluorescence to obtain fluorescence information corresponding to the fluorescence for detection. The imaging devices may be implemented in various possible ways. According to one possible implementation, each of the plurality of imaging devices includes an optical filter, an imaging lens, and a camera that are sequentially arranged, and for each imaging device, the optical filter thereof is positioned to filter the fluorescence guided to the imaging device by the fluorescence guiding device, and then transmit the filtered fluorescence to the imaging lens thereof, and the imaging lens thereof is positioned to focus the filtered fluorescence transmitted via the optical filter thereof on the camera thereof for imaging by the camera thereof to obtain fluorescence information corresponding to the fluorescence for detection. For each imaging device, including its lens and camera, the center thereof may be kept consistent with the transmission/reflection center of the element corresponding thereto in the fluorescence guiding device, for example, the second dichroic mirror guiding the corresponding fluorescence to the imaging device. The camera may be a TDI camera, which is suitable for TDI imaging.

[0052] A plurality of lasers of different wavelengths may be generated by at least one laser source, and the optical fiber may be positioned to receive the plurality of lasers of different wavelengths from the at least one laser source, and further to form and transmit laser(s) of a plurality of different wavelengths to the beam splitting device to achieve the incident laser(s) of a plurality of different wavelengths. The at least one laser source may be included in or outside the detecting apparatus.

[0053] Advantageously, the at least one laser source includes a plurality of laser sources, which may be used to generate the plurality of lasers of different wavelengths respectively.

[0054] In the embodiment shown in FIG. 1, advantageously, the beam splitting device 120 may be selected in such a manner that an included angle between emitting directions of excitation lasers of adjacent wavelengths among the plurality of excitation lasers emitted from the beam splitting device is not smaller than a threshold angle, such that a difference between incident angles at which the excitation lasers of adjacent wavelengths are incident on the first dichroic mirror is not smaller than a desired angle difference. The desired angular difference may be determined based on a ratio of a minimum spot spacing to a focal length of the objective

lens, e.g., is equal to or greater than the ratio of the minimum spot spacing to the focal length of the objective lens. The minimum spot spacing indicates a minimum distance at which focusing spots formed on the sample by the plurality of excitation lasers need to be spaced apart from one another, and may be suitably determined in various possible ways according to the situation. For example, the minimum spot spacing may be related to the requirements of a particular application and may be determined in advance based on the particular application at which the detecting apparatus is directed. For different detecting scenarios, detecting purposes, and/or samples to be detected, the required minimum spacing between the spots may vary. For example, the minimum spot spacing may be determined to satisfy the following conditions: being greater than a size in a corresponding direction of the spot formed on the surface of the sample by the plurality of coupled lasers from the optical fiber without dispersing the plurality of lasers (the size of the narrow side of the spot, i.e., the width of the spot; in the case of FIG. 1, being the size in the lateral direction of the spot shown); and the corresponding direction being a direction along which the spacing between the spaced apart spots is. In the case where the conditions are satisfied, it is advantageous that the value of the minimum spot spacing is as small as possible. Where the value of the minimum spot spacing is relatively large, some of the focused spots and imaging may exceed the range of the field of view of the objective lens, resulting in deterioration of the imaging. For example, in some cases, the minimum spot spacing may be determined to be equal to the height of the field of view of the imaging system on the sample in a particular application. As a simplified way, the threshold angle may be determined based on the ratio of the minimum spot spacing to the focal length of the objective lens. For example, the threshold angle may be determined to be equal to the ratio of the minimum spot spacing to the focal length of the objective lens multiplied by a coefficient, which may be predetermined to take into account considerations, for example, but being not limited to, whether the excitation lasers emitted from the beam splitting device need to undergo shaping/scaling before being received by the first dichroic mirror, the angular magnification that the excitation lasers emitted from the beam splitting device may need to undergo before being received by the first dichroic mirror, and the like. For example, the coefficient may be equal to 1, for example in the absence of a shaping device between the beam splitting device and the first dichroic mirror. As another

example, in the case where a shaping device is provided between the beam splitting device and the first dichroic mirror, the coefficient may be determined based on the angular magnification of the shaping device, for example, is equal to the reciprocal of the absolute value of the angular magnification.

[0055] Optionally, the detecting apparatus may include at least one of the following shaping devices: a first beam shaping device located between the optical fiber and the beam splitting device, and being positioned to shape the incident laser(s) of a plurality of different wavelengths output from the optical fiber, and to transmit the shaped incident laser(s) to the beam splitting device; and a second beam shaping device located between the beam splitting device and the first dichroic mirror, and being positioned to shape the plurality of excitation lasers corresponding to the plurality of different wavelengths of the incident laser(s) respectively and emitted from the beam splitting device, and to transmit the shaped plurality of excitation lasers to the first dichroic mirror. Each of the first beam shaping device and the second beam shaping device may be implemented in various possible ways. For example, the first beam shaping device may include a first lens group for performing desired shaping and scaling of an incident laser to be incident on the beam splitting device, for example but not limited to causing the incident laser to be incident on the beam splitting device in a manner of forming a spot of a desired shape and/or size; and the second beam shaping device may include a second lens group for performing desired shaping and scaling of an excitation laser emitted from the beam splitting device, for example but not limited to causing the excitation laser to be incident on the first dichroic mirror in a manner of forming a spot of a desired shape and/or size. In addition, for each of the first beam shaping device and the second beam shaping device, the angular magnification thereof can be appropriately determined according to the situation, and the particular composition and structure thereof can be designed based on the desired angular magnification thereof.

[0056] According to one possible implementation, the beam splitting device includes a single dispersion prism positioned in such a manner that each of the incident laser(s) of a plurality of different wavelengths from the optical fiber is incident on a first refractive surface of the single dispersion prism and each of the plurality of excitation light beams then exits from

a second refractive surface which is different from the first refractive surface, of the single dispersion prism. The incident angles at which the incident laser(s) of a plurality of different wavelengths is/are incident on the first refractive surface of the single dispersion prism may be different and need not to be fixed angles, and may be related to the orientation and placement angle of the single dispersion prism. Advantageously, the single dispersion prism may be positioned in such a manner that the incident laser(s) of a plurality of different wavelengths is/are incident on the first refractive surface of the single dispersion prism at a predetermined incident angle, the predetermined incident angle being selected in such a manner that a deviation angle between an incident direction of the incident laser incident on the first refractive surface and an exit direction of an excitation laser corresponding to the incident light exiting from the second refractive surface is minimized. The single dispersion prism may have a vertex angle formed between the first refractive surface and the second refractive surface, the first refractive surface and the second refractive surface are adjacent surfaces of the single dispersion prism, and the single dispersion prism is selected in such a manner that a combination of the vertex angle of the single dispersion prism and a material selected to form the single dispersion prism enables the included angle to be not smaller than the threshold angle. The single dispersion prism may be, for example, but is not limited to, a triangular prism, for example a right-angle prism having a vertex angle of 45 degrees and made of a material of N-SF11, a quadrangular prism, and the like. For example, in the case of a quadrangular prism being used, a certain angle of the quadrangular prism may be used as a vertex angle, and two adjacent refractive surfaces of the quadrangular prism that define this angle can be used as an incident surface for receiving a laser and an exit surface for outputting the laser respectively to refract the laser, which can be realized by appropriately placing the quadrangular prism. For a given single dispersion prism, the material, the vertex angle, and the like thereof are known, and the predetermined incident angle may be determined by related art means such as table lookup, calculation and the like. In addition, for a given single dispersion prism, for light of any wavelength incident on the prism at such a predetermined incident angle, the dispersive capability of the prism can be calculated by formulas and algorithms available in the related art (for example, "New Concept Physics Course-Optics" by Kaihua ZHAO). For the solution of the present disclosure, as a simplified

way, for the plurality of lasers used, light with a certain intermediate wavelength in the wavelength range of the plurality of lasers may be selected, and an amount of a change in the propagation direction of the selected light after the selected light is incident on a certain prism that can be selected at such a predetermined incident angle and refracted by the prism, that is, the minimum deviation angle of the selected light, is calculated; then, the prism with which the minimum deviation angle of the selected light being not smaller than the above threshold angle is satisfied may be determined as a prism that can be used.

[0057] According to another possible implementation, the beam splitting device includes a plurality of dispersion prisms. In this case, each of the plurality of dispersion prisms has a vertex angle formed between a first refractive surface and a second refractive surface thereof and is positioned to receive a laser incident thereon with the first refractive surface thereof and cause the laser to exit from the second refractive surface thereof, with a combination of a number of the plurality of dispersion prisms and a vertex angle and a material of each of the plurality of dispersion prisms being selected in such a manner that the included angle is not smaller than the threshold angle. Given the number, placement, and relative positional relation of the dispersion prisms, such a combination may be determined using relevant data, formulas, and algorithms available in the related art, as described above for a single prism. In this case, a first dispersion prism among the plurality of dispersion prisms that first receives the incident laser(s) of a plurality of different wavelengths from the optical fiber may be positioned in such a manner that each of the incident laser(s) of a plurality of different wavelengths from the optical fiber is incident on a first refractive surface of the first dispersion prism and then exits from a second refractive surface of the first dispersion prism, and each of the plurality of dispersion prisms other than the first dispersion prism may be positioned in such a manner that each of the laser(s) exiting from an previous dispersion prism adjacent thereto is incident on a first refractive surface thereof and exits from a second refractive surface thereof. As compared with using a single dispersion prism, when a plurality of dispersion prisms are used, the direction of optical path will be more flexible, and there will be less restriction on the placement position or angle of other components in the detecting apparatus, but the transmittance of laser will be lower when the plurality of dispersion prisms are used. Therefore, in a particular application, one can choose

to use a single dispersion prism or a plurality of dispersion prisms according to the actual needs.

[0058] As mentioned above, the beam splitting device may also be realized by grating(s). In the case of grating(s) being used, an appropriate combination of the orientation, position, and possible number of the grating(s), etc., may be determined by data (type, parameters, structure, etc. of available gratings), formulas (basic formulas for grating diffraction, etc.), algorithms, etc., available in the related art, such that the beam splitting device satisfies the above-mentioned relevant requirements.

[0059] Herein, use of the terms "front"/"rear", "before"/"after", "preceding"/"following", "previous"/"next" is based on the propagation direction of light. For example, in the case where the same light beam propagates through multiple components, a component that the light beam passes through first during propagation of the light beam may be called a front component, a preceding component, or a previous component relative to a component that the light beam passes through later during propagation of the light beam.

[0060] The detecting apparatus of the present disclosure is not limited to using laser(s) from an optical fiber as described in the above embodiment, but may use excitation light from various other light sources, such as light emitted by an LED light source, light emitted by a halogen light source, and the like.

[0061] As shown in FIG. 2, a detecting apparatus 20 according to another embodiment of the present disclosure includes the following components: a multimode optical fiber 210, a first beam shaping device 270, a laser filter 290, a dispersion prism 220, a second beam shaping device 280, a dichroic mirror 1 230, an objective lens 240, dichroic mirror 2 to dichroic mirror i+1 and optical filter 1 to optical filter i constituting a fluorescence guiding device 250, and imaging lens 1 to imaging lens i and camera 1 to camera i constituting an imaging system 260, where i represents the type/number of lasers of different wavelengths coupled through the multimode optical fiber, and is an integer greater than 1. It should be understood that for the purpose of clarity and simplification, only lasers of three wavelengths are shown in FIG. 2 to schematically represent lasers of i wavelengths, and the present disclosure is not limited to being only applied to the case of lasers of three wavelengths, but may be applied to the case of lasers of more or fewer wavelengths.

[0062] As shown in FIG. 2, the detecting apparatus uses the multimode fiber 210 to coaxially couple i lasers of different wavelengths ($i \geqslant 2$) and then outputs a coupled laser of different wavelengths through the multimode fiber, and the coupled laser is shaped as to the optical path by the first beam shaping device 270, filtered by the laser filter 290, and then incident on a first refractive surface of the dispersion prism 220. According to the law of refraction, the lasers of different wavelengths have different refractive indexes, that is, different refractive angles. Therefore, the lasers of different wavelengths, after being refracted by the first refractive surface of the dispersion prism, will have different propagation angles, and after the lasers of different wavelengths are further refracted by the second refractive surface of the dispersion prism, the difference between the propagation angles of the lasers of different wavelengths will be enlarged. In this way, an included angle greater than zero will be produced between the transmission directions of the lasers of different wavelengths. Generally, the shorter the wavelength of a laser, the greater its corresponding refractive index and refractive angle. After dispersion by the dispersion prism, the i lasers with different propagation angles (schematically shown in FIG. 2 by laser 1, laser 2, and laser i) are reflected by the dichroic mirror 1 230 and focused by the objective lens 240 and then irradiate on the surface of a sample 200. Since the lasers each have different propagation angles, the lasers each form their own spots (schematically shown in FIG. 2 by spot 1, spot 2, and spot i) and irradiate at different positions of the sample, and the laser spot at each of the positions irradiated by the lasers on the sample originates from a laser of a single wavelength.

[0063] In order to clearly illustrate the operating process of the detecting apparatus shown in FIG. 2, here assuming that i=3, the apparatus is further exemplified by taking an example of the apparatus using a multimode fiber to couple three lasers of A, B and C (not shown). A coupled laser formed by the three lasers of A, B and C is reflected by the dichroic mirror 1 230 and focused by the objective lens 240 and then irradiate at different positions on the surface of the sample, and at a certain point in time, the three lasers of A, B and C have illumination areas a, b, and c (not shown) on the sample respectively, and excite fluorescence AX, BX and CX (not shown) correspondingly in the areas a, b, and c respectively. Assuming that the area c is foremost, the area a is rearmost, and the area b is in the middle in the moving direction of the sample, the

sample scanning direction is the same as the advancing direction of the illumination area (currently, the area a) of the laser A. The three lasers of A, B and C excite fluorescence simultaneously, and at each point in time, only one fluorescence is excited and emitted at each position on the sample that is illuminated. At the next point in time after the sample is moved, the laser A excites fluorescence AX' in a new area, the laser B excites fluorescence BX' in the area a, and the laser C excites fluorescence CX' in the area b. By proceeding back and forth in this way, the scanning of the whole sample can be completed. During the scanning of the sample, all the fluorescence excited at the same time is transmitted to the dichroic mirror 1 via the objective lens, then transmitted to the dichroic mirror 2, guided and filtered via the dichroic mirror 2 to dichroic mirror 4 and the optical filter 1 to optical filter 3, and then imaged by the imaging lens 1 to imaging lens 3 to the camera 1 to camera 3. For example, the dichroic mirror 2 is selected to transmit one of the fluorescence AX, BX, CX transmitted thereto, for example the fluorescence AX, to guide it to the corresponding optical filter 1, and to reflect the remaining fluorescence, for example the fluorescence BX and CX, to the dichroic mirror 3; the dichroic mirror 3 is selected to reflect one of the fluorescence BX and CX transmitted thereto, for example the fluorescence BX, to guide it to the corresponding optical filter 2, and to transmit the remaining fluorescence, for example the fluorescence CX, to the dichroic mirror 4; and the dichroic mirror 4 is selected to reflect the fluorescence transmitted thereto, for example the fluorescence CX, to guide it to the corresponding optical filter 3. Correspondingly, the optical filter 1 may be selected to allow only the fluorescence AX to pass through it to reach the corresponding imaging lens 1; the optical filter 2 may be selected to allow only the fluorescence BX to pass through it to reach the corresponding imaging lens 2; and the optical filter 3 may be selected to allow only the fluorescence CX to pass through it to reach the corresponding imaging lens 3. In this way, different fluorescence excited at the same time corresponds to the camera 1 to camera 3 in a one-to-one correspondence; besides, the fluorescence is excited at different positions on the sample individually, and different fluorescence is separated and captured by different cameras.

[0064] Assuming that lasers of n wavelengths are coaxially coupled using a multimode fiber, the duration of single-channel fluorescence detection of each FOV is T, the power of each laser

is Wi, and the area of a laser spot on the sample is Si, in the case of the above first related art being adopted, the laser irradiation power density to which a unit area of the sample is subjected is $\rho = \sum_1^n Wi/Si$; assuming that $Wi=W$, $Si=S$, then $\rho = nW/S$. According to the operating process as described above, in the case of the technical solution of the present disclosure being adopted, the laser irradiation power density to which a unit area of the sample is subjected is $\rho' = W/S = \rho/n$, i.e., the laser power density is reduced to 1/n of its original value. Moreover, when the technical solution of the present disclosure is adopted, all the fluorescence can be excited simultaneously and photographed by the cameras at the same time to obtain the fluorescence detection information, and therefore the detection duration of a single FOV is equal to the detection duration T for a single fluorescence in the case of the related art.

[0065] For the detecting apparatus shown in FIG. 2, the dispersion prism thereof may be suitably placed at various possible angles and orientations. The placement of the dispersion prism may be determined based at least in part on the dichroic mirror 1, for example, such that the exit angle of an excitation laser that exits from the dispersion prism after being refracted by the dispersion prism conforms to the range of angles of incident light beam that the dichroic mirror 1 is designed to require. With respect to the selection of the dispersion prism (e.g., a material, a vertex angle, etc. of the prism), further exemplary illustration will be given below. Assuming that the focal length of the objective lens in the detecting apparatus is represented by f and the minimum required distance by which the spots formed by different lasers on the sample need to be separated (i.e., the minimum spot spacing) is represented by d, where the approximating condition that "the objective lens is a thin lens and the field of view of the objective lens is <5°" is satisfied, it can be determined that the minimum required angle at which lasers of adjacent wavelengths incident on the dichroic mirror 1 need to be separated is $\Delta\theta_T \approx d/f$, and this angle $\Delta\theta_T$ may be referred to as a first threshold angle. The dispersive capability of a prism is determined by the material, the size of the vertex angle (the included angle formed by the incident surface and the exit surface of the prism) and the like of the prism. Taking an example of the dispersion prism being a triangular prism, assuming that lasers are incident on the first refractive surface of the triangular prism in the direction that produces the minimum deviation angle, the angle $\Delta\theta_T$ can be calculated based on the distance d. With $\Delta\theta_T$ determined,

it is possible to determine the condition that the included angle between excitation lasers of adjacent wavelengths exiting from the dispersion prism needs to satisfy, that is, the included angle needing to be not smaller than a second threshold angle $\Delta\theta_T$', which can be determined by, for example, considering the angular magnification of the second beam shaping device provided between the beam splitting device and the dichroic mirror 1 and based on the angle $\Delta\theta_T$ and the angular magnification, e.g., $\Delta\theta_T$' may be equal to the first threshold angle divided by the absolute value of the angular magnification. A suitable prism may then be selected from available prisms based on the prism dispersion equation in such a manner that the material and the vertex angle of the selected prism enable the included angle between excitation lasers of adjacent wavelengths exiting from the prism to satisfy the relevant requirements. Specifically, it is known from the principles of geometric optics that when a laser is incident on a prism in a direction that produces the minimum deviation angle, the resulting laser image is minimally curved (i.e., the aberration is minimized), and for a laser incident at this incident angle, the angular dispersive ability of the prism, D_θ, is shown by equation (1):

[0066]
$$D_\theta = \frac{2\sin(\alpha/2)}{\sqrt{1-n^2\sin^2(\alpha/2)}}\frac{dn}{d\lambda} = \frac{b}{a}\frac{dn}{d\lambda} \quad (1)$$

[0067] where α represents a vertex angle of the prism, n represents the refractive index of the prism (determined by the material of the prism), λ represents the wavelength of the laser; $dn/d\lambda$ represents the dispersive index of the prism, b represents the length of the bottom edge of the prism, and a represents the width of the beam (related to the specific application; different applications require different beam widths).

[0068] A detecting apparatus 30 according to yet another embodiment of the present disclosure is shown in FIG. 3. Hereinafter, the detecting apparatus of the present disclosure is further exemplarily described by taking an example in which lasers of two wavelengths enter the detecting apparatus shown in FIG. 3 via a coaxial coupled optical fiber, the beam shaping device includes a first illumination lens group 370 and a second illumination lens group 380, and the dispersion prism is a triangular prism 320. The first illumination lens group and the second illumination lens group are combined to form a shaping and scaling system. The dichroic mirror group 330 may correspond, in function and structure, to a combination of the first

dichroic mirror and the fluorescence guiding device in FIG. 1 or the dichroic mirror 1 to dichroic mirror i+1 in FIG. 2. The triangular prism is a 45° dispersion prism. An optical path is located in a YZ plane and a sample plane 300 of the sample to be irradiated by the lasers is perpendicular to the YZ plane.

[0069] Lasers of two wavelengths, i.e., a green laser and a red laser, are output through a coaxial coupled optical fiber 310. After being shaped by the first illumination lens group 370 and refracted sequentially by a first refractive surface 3201 of the prism 320 and a second refractive surface 3202 of the prism 320, main light beams of the two lasers form an included angle therebetween. The light beams are shaped further by the second illumination lens group 380, and a final included angle between center light beams of the two lasers exiting from the second illumination lens group needs to be not smaller than the above threshold angle $\Delta\theta_T$. The main light beams of the two lasers with different exiting angles are transmitted to an objective lens 340 via dichroic mirrors in the dichroic mirror group 330 and are focused and imaged on the sample by the objective lens, and spots of the two lasers are formed at different positions on the sample and are separated on the sample. On the other hand, fluorescence excited on the sample by the lasers is received by the objective lens 340, and split and guided to an imaging system 360 for imaging by the dichroic mirrors in the dichroic mirror group 330.

[0070] The difference between the center wavelengths of the green laser and the red laser is 128nm, and the height of the field of view of the imaging system on the sample is 80μm. Here, a "center wavelength" may be understood as a peak wavelength of a laser. In order to keep the spots of the lasers on the sample separate and non-interfering with each other, the distance between the spots of lasers of adjacent wavelengths on the sample can be preset to be greater than 80μm. The focal length of the objective lens is known, and assuming that the maximum angle of view of the objective lens in the light splitting direction is <5°, i.e., the approximating condition is satisfied, it is determined according to the method described above that $\Delta\theta_T$=0.4°, that is, the included angle $|\Delta\theta|$ between the center light beams of lasers of adjacent wavelengths exiting from the second illumination lens group needs to be greater than 0.4°.

[0071] In the YZ plane as shown in FIG. 3, at an approximately central position between the first illumination lens group and the second illumination lens group, the beam diameter of the

lasers is approximately 13.5 mm. The distance of the central position from the first illumination lens group is related to the size of the optical fiber and the focal length of the first illumination lens group. Assuming that in this embodiment the central position is about 50mm from the first illumination lens group and after the first illumination lens group, the beam diameter is a beam diameter of the lasers exiting from the first illumination lens group at about 50mm after the first illumination lens group. The second illumination lens group is similar to a telescope in principle, and its angular magnification is M2=-0.7, and by calculation according to the approximating condition (i.e., the objective lens is approximated as a thin lens, and the angle of view of the objective lens is <5°), it can be drawn that the angular difference $|\Delta\theta'|$ between the center light beams of lasers of different wavelengths exiting from the prism and arriving at the second illumination lens group needs to satisfy inequation (2):

[0072] $$|\Delta\theta'| \geq |\Delta\theta|/|M_2| \approx 0.57° \quad (2)$$

[0073] In the present embodiment, a prism having a vertex angle of 45° and made of a material of N-SF11 is selected. Since an amount of change in dispersive index of most optical materials does not exceed one order of magnitude within the selected laser wavelengths, the dispersive index $|D_\theta|$ of the prism may be calculated for the center wavelength 596nm within the wavelength range of the selected red laser and green laser, and then the so-calculated dispersive index is utilized to judge whether the angular difference between the red laser and green laser used when exiting from the prism satisfies the relevant requirements, thus judging whether the selected prism conforms to the requirements. Specifically, after table lookup and calculation, the following can be obtained:

[0074] $$\lambda = 596nm \Rightarrow \frac{dn}{d\lambda} \approx -1.78 \times 10^{-4}(nm^{-1}) \quad (3)$$

[0075] $$|D_\theta| \approx 0.009°/nm \quad (4)$$

[0076] $$\frac{|\Delta\theta'|}{\Delta\lambda} = 0.57°/128nm = 0.0045°/nm \quad (5)$$

[0077] where $\Delta\lambda$ represents the wavelength difference between the red laser and the green laser. By equations (4) and (5), it can be obtained that $|D_\theta| > |\Delta\theta'|/\Delta\lambda$, i.e., the selected prism satisfies the requirements of the dispersive angle of the present embodiment.

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[0078] After the material and the vertex angle of the prism are determined, the incident angle of the lasers to the prism may be adjusted to satisfy the condition of the minimum deviation angle. For the embodiment, it is known through calculation that the condition of the minimum deviation angle is satisfied when the incident angle is 43.1°. After optical simulation, it is obtained that the included angle between the main light beams of the lasers of two wavelengths after dispersion by this prism is 1.2°, and when finally reaching the objective lens, the main light beams of the red laser and the green laser form therebetween an included angle of 0.82°, which is > 0.57°, that is, the requirements are satisfied. Finally, the spot distance between the spot formed by the red laser and the spot formed by the green laser on the sample is about 0.16mm. The simulation result is shown in FIG. 4, in which a strip-shaped spot at the upper part is the spot 4001 formed by the red laser, the strip-shaped spot at the lower part is the spot 4002 formed by the green laser, and the centers of the red spot and the green spot are separated by a distance of about 0.16mm.

[0079] The present embodiment uses the TDI imaging technology, and when each laser is turned on, the corresponding camera is triggered to take images, and the camera integration process when the sample is scanned by the system is shown in FIG. 5. In the process of fluorescence excitation, the red laser and the green laser excite different areas of the sample respectively, and the excitation areas of the laser spots on the sample correspond to the corresponding cameras in a one-to-one correspondence in terms of the object-image relation. Assuming that the red laser corresponds to camera A and the green laser corresponds to camera B. With the TDI imaging technology, the camera integration direction is along the narrow side of the spots, and fluorescence excitation is sequential. When a laser excites the sample, the camera integration is triggered synchronously, that is, the triggering interval between the camera triggering sources corresponding to the red laser and the green laser is equal to the time interval required for a spot to move a distance of 0.16mm relative to the sample (the spot is fixed and the sample is driven by a sliding table located in the XY plane to move). When the green laser enters the sample area, it starts to excite fluorescence, and at the same time, the integration of the camera B starts, and the camera A waits at this time; when the red laser enters the sample, the integration of the camera A starts, and the camera B is integrating at this time; when the

green laser leaves the sample, the integration of the camera B ends, and the camera A is still integrating; and the red laser leaves the sample, the integration of the camera A ends, and the fluorescence detection of this row of the sample is completed. Since the time required to move the sample by 0.16 mm is much shorter than the integration duration for a single row, the duration required for all fluorescence detection of the single row is almost equal to the duration of single-channel fluorescence detection. When entering the next row, the red laser and the green laser enter the sample in an opposite order, and integrate in an opposite order. In this way, the scanning detection of the whole sample is completed.

[0080] The present disclosure may also be implemented as a detecting system, for example but not limited to a gene sequencing system, including the detecting apparatus as described above. In the case of the gene sequencing system, the imaging system of the detecting apparatus of the present disclosure is used to collect a fluorescent signal on a sequencing chip as a sample to be detected.

[0081] FIG. 8a shows a relation between a data quality Q30 and a read length for gene detection results obtained by performing a double-end test on a test object, i.e., DNA sequences, using the first related art (i.e. simultaneous excitation), using the second related art (i.e., time-division excitation), and using the present disclosure. FIG. 8b shows a relation between a detection error rate and a read length for gene detection results obtained by performing a double-end test on the test object, i.e., DNA sequences, using the first related art (i.e. simultaneous excitation), using the second related art (i.e., time-division excitation), and using the present disclosure. The first related art, the second related art, and the present disclosure are respectively configured for gene detection under the same conditions. In FIG. 8a and FIG. 8b, a dashed line represents a detection result obtained by using the first related art, a hollow line ("time-division excitation 1") represents a detection result obtained by using the second related art, and a solid line ("the present disclosure") represents a detection result obtained by using the present disclosure. In order to compare the technical effects of the first related art, the second related art and the present disclosure, the Q30 and the detection error rate (i.e., the error rate in identifying bases) in the gene detection results are used as evaluation indexes; the higher the Q30, and the lower the detection error rate, the better and the more accurate the detection result is. As can be

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seen from FIG. 8a and FIG. 8b, the difference between the starting results of the two related arts and the present disclosure at smaller read lengths is very small, but for the first related art, both Q30 and the detection error rate get worse as the read length increases (in general characterized by increasingly smaller Q30 and increasingly higher detection error rate), and for the second related art and the present disclosure, the magnitude of deterioration in Q30 and detection error rate is smaller than that in the case of the first related art; in addition, for both the present disclosure and the second related art, both Q30 and the detection error rate are very close overall, and are the same or substantially the same at some read lengths. Therefore, as far as the gene sequencing results are concerned, the second related art and the present disclosure are similar and both are significantly better than the first related art, but the second related art is doubled as to the time consumed for photographing as compared with the first related art, whereas the detection duration required with the present disclosure is the same as that in the case of the first related art.

[0082] The solution of the present disclosure can be applied for various applications requiring fluorescence excitation and fluorescence detection, and is especially suitable for biochemical detection, such as gene detection or other cases requiring exciting of a sample to generate fluorescence and detecting of the excited fluorescence.

[0083] The technical means used by the present disclosure in order to achieve the intended purpose and the effect thereof should be more deeply and specifically understood by the detailed description of the specific embodiments; however, the accompanying drawings are merely for reference and illustration, and are not intended to limit the present disclosure.

CLAIMS

What is claimed is:

1. A detecting apparatus, comprising a beam splitting device, a first dichroic mirror, an objective lens, a fluorescence guiding device, and an imaging system comprising a plurality of imaging devices, wherein,

the beam splitting device is configured to receive and separate an incident light beam of a plurality of different wavelengths from an optical fiber, to form a plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam emitted in different emitting directions from the beam splitting device, wherein, each of the excitation light beams has a wavelength in a one-to-one correspondence with the plurality of different wavelengths of the incident light beam;

the first dichroic mirror is positioned to receive the plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam in a one-to-one correspondence and emitted from the beam splitting device, to transmit the plurality of excitation light beams to the objective lens, such that the plurality of excitation light beams are focused respectively on a plurality of different areas of a sample to be detected through the objective lens, to excite a plurality of fluorescence in the plurality of different areas of the sample on which the plurality of excitation light beams are focused respectively, and to receive the plurality of fluorescence excited by the plurality of excitation light beams respectively and transmit the plurality of fluorescence to the fluorescence guiding device;

the objective lens is positioned to receive the plurality of excitation light beams transmitted by the first dichroic mirror, to focus the plurality of excitation light beams on the plurality of different areas of the sample respectively, and to transmit the plurality of fluorescence excited by the plurality of excitation light beams respectively to the first dichroic mirror;

the fluorescence guiding device is positioned to receive the plurality of fluorescence transmitted by the first dichroic mirror, and to guide the plurality of fluorescence to the plurality of imaging devices respectively, such that each fluorescence of the plurality of fluorescence is imaged by one of the plurality of imaging devices corresponding to the

fluorescence; and

each of the plurality of imaging devices is positioned to receive one fluorescence of the plurality of fluorescence guided by the fluorescence guiding device, and to image the fluorescence to obtain fluorescence information corresponding to the fluorescence for detection.

2. The detecting apparatus according to claim 1, further comprising:

at least one light source configured to generate a plurality of excitation light of different wavelengths,

wherein the optical fiber is positioned to receive the plurality of excitation light of different wavelengths from the at least one light source, and to form the incident light beam of a plurality of different wavelengths and transmit the incident light beam of a plurality of different wavelengths to the beam splitting device.

3. The detecting apparatus according to claim 2, wherein the at least one light source comprises a plurality of light sources for generating the plurality of excitation light of different wavelengths respectively.

4. The detecting apparatus according to claim 1, wherein the beam splitting device is selected in such a manner that an included angle between emitting directions of excitation light beams of adjacent wavelengths among the plurality of excitation light beams emitted from the beam splitting device is not smaller than a threshold angle.

5. The detecting apparatus according to claim 4, wherein the threshold angle is based on a ratio of a predetermined minimum spacing to a focal length of the objective lens, the predetermined minimum spacing indicating a minimum distance at which focusing spots formed on the sample by the plurality of excitation light beams need to be spaced apart from one another.

6. The detecting apparatus according to any one of claims 1 to 5, further comprising at least one of:

a first beam shaping device located between the optical fiber and the beam splitting device, and being positioned to shape the incident light beam of a plurality of different wavelengths output from the optical fiber, and to transmit shaped incident light beam to the beam splitting device; and

a second beam shaping device located between the beam splitting device and the first

dichroic mirror, and being positioned to shape the plurality of excitation light beams corresponding to the incident light of a plurality of different wavelengths in a one-to-one correspondence and emitted from the beam splitting device, and to transmit shaped plurality of excitation light beams to the first dichroic mirror.

7. The detecting apparatus according to claim 6 when it depends on claim 5, wherein the second beam shaping device has an angular magnification, and in the case where the detecting apparatus comprises the second beam shaping device, the threshold angle is equal to a product of the ratio of the predetermined minimum spacing to the focal length of the objective lens and a reciprocal of an absolute value of the angular magnification.

8. The detecting apparatus according to claim 6, wherein the first beam shaping device comprises a first lens group, and the second beam shaping device comprises a second lens group.

9. The detecting apparatus according to claim 4 or 5, wherein the beam splitting device comprises at least one dispersion prism.

10. The detecting apparatus according to claim 9, wherein the at least one dispersion prism comprises a single dispersion prism positioned in such a manner that the incident light beam of a plurality of different wavelengths from the optical fiber is incident on a first refractive surface of the single dispersion prism and each of the plurality of excitation light beams then exits from a second refractive surface which is different from the first refractive surface, of the single dispersion prism.

11. The detecting apparatus according to claim 10, wherein the incident light beam of a plurality of different wavelengths is incident on the first refractive surface of the single dispersion prism at a predetermined incident angle, the predetermined incident angle being selected in such a manner that a deviation angle between an incident direction of the incident light beam incident on the first refractive surface and an exit direction of the plurality of excitation light beams corresponding to the incident light beam and exiting from the second refractive surface is minimized.

12. The detecting apparatus according to claim 10, wherein the first refractive surface and the second refractive surface are adjacent surfaces of the single dispersion prism, the single dispersion prism has a vertex angle formed between the first refractive surface and the second refractive surface, and the single dispersion prism is selected in such a manner

that a combination of the vertex angle of the single dispersion prism and a material selected to form the single dispersion prism enables the included angle to be not smaller than the threshold angle.

13. The detecting apparatus according to claim 12, wherein the single dispersion prism is a right-angle prism having a vertex angle of 45 degrees and made of a material of N-SF11.

14. The detecting apparatus according to claim 12, wherein the single dispersion prism is a triangular prism.

15. The detecting apparatus according to claim 9, wherein the at least one dispersion prism comprises a plurality of dispersion prisms that are sequentially arranged, each of the plurality of dispersion prisms having a vertex angle formed between a first refractive surface and a second refractive surface thereof that are adjacent and being positioned to receive each light incident thereon with the first refractive surface thereof and cause the light to exit from the second refractive surface thereof, wherein a combination of a number of the plurality of dispersion prisms and a vertex angle and a material of each of the plurality of dispersion prisms is selected in such a manner that the included angle is not smaller than the threshold angle.

16. The detecting apparatus according to claim 15, wherein a first dispersion prism among the plurality of dispersion prisms that first receives the incident light beam of a plurality of different wavelengths from the optical fiber is positioned in such a manner that the incident light beam of a plurality of different wavelengths from the optical fiber is incident on a first refractive surface of the first dispersion prism and then exits from a second refractive surface of the first dispersion prism, and each of the plurality of dispersion prisms other than the first dispersion prism is positioned in such a manner that each of light exiting from an previous dispersion prism adjacent thereto is incident on a first refractive surface thereof and exits from a second refractive surface thereof.

17. The detecting apparatus according to claim 4, wherein the beam splitting device comprises at least one grating.

18. The detecting apparatus according to claim 1, wherein the fluorescence guiding device comprises a plurality of second dichroic mirrors that are sequentially arranged, the plurality of second dichroic mirrors comprising a last second dichroic mirror that is away from the first dichroic mirror and at least one preceding second dichroic mirror located

between the last second dichroic mirror and the first dichroic mirror, the plurality of fluorescence received by the first dichroic mirror propagating sequentially through the plurality of second dichroic mirrors;

each preceding second dichroic mirror of the preceding second dichroic mirror(s) is positioned to guide one of at least one fluorescence incident thereon among the plurality of fluorescence to the imaging device corresponding to the preceding second dichroic mirror, and to guide remaining fluorescence of the at least one fluorescence to a next second dichroic mirror adjacent to the preceding second dichroic mirror; and

the last second dichroic mirror is positioned to guide fluorescence incident thereon to the imaging device corresponding to the last second dichroic mirror.

19. The detecting apparatus according to claim 18, wherein the second dichroic mirror located closest to the first dichroic mirror among the at least one preceding second dichroic mirror is selected to transmit the fluorescence that is guided thereby to the imaging device corresponding thereto and reflect remaining fluorescence of the plurality of fluorescence incident thereon to a next second dichroic mirror that is adjacent thereto, the last second dichroic mirror is selected to guide the fluorescence incident thereon to the imaging device corresponding to the last second dichroic mirror through reflection; and for each of the second dichroic mirror(s) in the plurality of second dichroic mirrors other than the second dichroic mirror located closest to the first dichroic mirror and the last second dichroic mirror, the second dichroic mirror is selected to reflect the fluorescence that is guided by it to the imaging device corresponding to it and transmit remaining fluorescence of the at least one fluorescence incident thereon to a next second dichroic mirror that is adjacent to it.

20. The detecting apparatus according to claim 18, wherein the second dichroic mirror located closest to the first dichroic mirror among the at least one preceding second dichroic mirror is selected to reflect the fluorescence that is guided thereby to the imaging device corresponding thereto and transmit remaining fluorescence of the plurality of fluorescence incident thereon to a next second dichroic mirror that is adjacent thereto, the last second dichroic mirror is selected to guide the fluorescence incident thereon to the imaging device corresponding to the last second dichroic mirror through reflection; and for each of the second dichroic mirror(s) in the plurality of second dichroic mirrors other than the second dichroic mirror located closest to the first dichroic mirror and the last second dichroic mirror,

the second dichroic mirror is selected to reflect the fluorescence that is guided by it to the imaging device corresponding to it and transmit remaining fluorescence of the at least one fluorescence incident thereon to a next second dichroic mirror that is adjacent to it.

21. The detecting apparatus according to claim 1, wherein each imaging device comprises an optical filter, an imaging lens, and a camera that are sequentially arranged, and for each imaging device,

the optical filter thereof is positioned to filter the fluorescence guided to the imaging device by the fluorescence guiding device, and then transmit filtered fluorescence to the imaging lens thereof; and

the imaging lens thereof is positioned to focus the filtered fluorescence transmitted via the optical filter thereof on the camera thereof for imaging by the camera thereof to obtain fluorescence information corresponding to the fluorescence for detection.

22. The detecting apparatus according to any one of claims 1-5 and 18-21, wherein the optical fiber is a single optical fiber.

23. The detecting apparatus according to claim 22, wherein the single optical fiber is a coaxial coupled optical fiber.

24. The detecting apparatus according to any one of claims 1-5 and 18-21, wherein the sample is a biological sample or a chemical sample.

25. The detecting apparatus according to any one of claims 1-5 and 18-21, being a gene detecting apparatus.

26. A gene sequencing system, comprising an imaging system for collecting a fluorescence signal on a sequencing chip; and an optical system located between the imaging system and the sequencing chip, characterized in that the optical system comprises:

a light source configured to emit an incident light beam of a plurality of different wavelengths;

a beam splitting device configured to receive and separate the incident light beam of a plurality different wavelengths from the light source, to form a plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam emitted in different emitting directions from the beam splitting device, wherein, each of the excitation light beams has a wavelength in a one-to-one correspondence with the plurality of different wavelengths of the incident light beam;

a first dichroic mirror configured to receive the plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam in a one-to-one correspondence and emitted from the beam splitting device;

an objective lens arranged between the sequencing chip and the first dichroic mirror and configured to receive the plurality of excitation light beams transmitted by the first dichroic mirror, to focus the plurality of excitation light beams on a plurality of different areas on the sequencing chip to excite a plurality of fluorescence in the plurality of different areas in one-to-one correspondence with the plurality of excitation light beams respectively, and to transmit the plurality of fluorescence to the first dichroic mirror; and

a fluorescence guiding device configured to receive the plurality of fluorescence transmitted via the first dichroic mirror and to guide the plurality of fluorescence to the imaging system respectively,

wherein the imaging system comprises a plurality of imaging devices corresponding to the plurality of fluorescence in a one-to-one correspondence, each of the plurality of imaging devices being configured to receive one fluorescence, which corresponds to the imaging device, of the plurality of fluorescence guided by the fluorescence guiding device, and to image the fluorescence to obtain fluorescence information corresponding to the fluorescence.

27. The gene sequencing system according to claim 26, the beam splitting device is selected in such a manner that an included angle between emitting directions of excitation light beams of adjacent wavelengths in the plurality of excitation light beams emitted from the beam splitting device is not smaller than a threshold angle.

28. The gene sequencing system according to claim 27, wherein the threshold angle is based on a ratio of a predetermined minimum spacing to a focal length of the objective lens, the predetermined minimum spacing indicating a minimum distance at which focusing spots formed on the sequencing chip by the plurality of excitation light beams need to be spaced apart from one another.

29. The gene sequencing system according to any one of claims 26-28, wherein the optical system further comprises at least one of:

a first beam shaping device located between the light source and the beam splitting device, and being positioned to shape the incident light beam of a plurality of different

wavelengths output from the light source and to transmit shaped incident light beam to the beam splitting device; and

a second beam shaping device located between the beam splitting device and the first dichroic mirror, and being positioned to shape the plurality of excitation light beams corresponding to the incident light beam of a plurality of different wavelengths in a one-to-one correspondence and emitted from the beam splitting device and to transmit shaped plurality of excitation light beams to the first dichroic mirror.

30. The gene sequencing system according to claim 29 when it depends on claim 28, wherein the second beam shaping device has an angular magnification, and in the case where the optical system comprises the second beam shaping device, the threshold angle is equal to a product of the ratio of the predetermined minimum spacing to the focal length of the objective lens and a reciprocal of an absolute value of the angular magnification.

31. The gene sequencing system according to any one of claims 26-28, wherein the beam splitting device comprises at least one dispersion prism.

32. The gene sequencing system according to claim 31 when it depends on claim 27, wherein the at least one dispersion prism comprises a single dispersion prism positioned in such a manner that the incident light beam of a plurality of different wavelengths from the light source is incident on a first refractive surface of the single dispersion prism and each of the plurality of excitation light beams then exits from a second refractive surface which is different from the first refractive surface, of the single dispersion prism.

33. The gene sequencing system according to claim 32, wherein the incident light beam of a plurality of different wavelengths is incident on the first refractive surface of the single dispersion prism at a predetermined incident angle, the predetermined incident angle being selected in such a manner that a deviation angle between an incident direction of the incident light beam incident on the first refractive surface and an exit direction of the plurality of excitation light beams corresponding to the incident light beam and emitting from the second refractive surface is minimized.

34. The gene sequencing system according to claim 32, wherein the first refractive surface and the second refractive surface are adjacent surfaces of the single dispersion prism, the single dispersion prism has a vertex angle formed between the first refractive surface and the second refractive surface, and the single dispersion prism is selected in such a

manner that a combination of the vertex angle of the single dispersion prism and a material selected to form the single dispersion prism enables the included angle to be not smaller than the threshold angle.

35. The gene sequencing system according to claim 34, wherein the single dispersion prism is a triangular prism.

36. The gene sequencing system according to claim 31 when it depends on claim 27, wherein the at least one dispersion prism comprises a plurality of dispersion prisms that are sequentially arranged, each of the plurality of dispersion prisms having a vertex angle formed between a first refractive surface and a second refractive surface thereof that are adjacent and being positioned to receive each light incident thereon with the first refractive surface thereof and cause the light to exit from the second refractive surface thereof, wherein a combination of a number of the plurality of dispersion prisms and a vertex angle and a material of each of the plurality of dispersion prisms is selected in such a manner that the included angle is not smaller than the threshold angle.

37. The gene sequencing system according to claim 36, wherein a first dispersion prism among the plurality of dispersion prisms that first receives the incident light beam of a plurality of different wavelengths from the light source is positioned in such a manner that the incident light beam of a plurality of different wavelengths from the light source is incident on a first refractive surface of the first dispersion prism and then exits from a second refractive surface of the first dispersion prism, and each dispersion prism of the plurality of dispersion prisms other than the first dispersion prism is positioned in such a manner that each of light exiting from an previous dispersion prism adjacent to the dispersion prism is incident on a first refractive surface of the dispersion prism and then exits from a second refractive surface of the dispersion prism.

38. The gene sequencing system according to any one of claims 26-28, wherein the beam splitting device comprises at least one grating.

39. The gene sequencing system according to claim 26, wherein the fluorescence guiding device comprises a plurality of second dichroic mirrors that are sequentially arranged, the plurality of second dichroic mirrors comprising a last second dichroic mirror that is away from the first dichroic mirror and at least one preceding second dichroic mirror located between the last second dichroic mirror and the first dichroic mirror, the plurality

of fluorescence received by the first dichroic mirror propagating sequentially through the plurality of second dichroic mirrors;

each preceding second dichroic mirror of the preceding second dichroic mirror(s) is positioned to guide one of at least one fluorescence incident thereon among the plurality of fluorescence to the imaging device corresponding to the preceding second dichroic mirror, and to guide remaining fluorescence of the at least one fluorescence to a next second dichroic mirror adjacent to the preceding second dichroic mirror; and

the last second dichroic mirror is positioned to guide fluorescence incident thereon to the imaging device corresponding to the last second dichroic mirror.

40. The gene sequencing system according to any one of claims 26-28 and 39, wherein the light source is a laser source or an LED light source.

41. The gene sequencing system according to claim 40, wherein the incident light beam is formed by lasers emitted by the laser source which are adapted to be transmitted directly to the beam splitting device or to be transmitted to the beam splitting device via an optical fiber.

42. A detecting method, comprising:

emitting, by a light source or a light conduction device, an incident light beam of a plurality of different wavelengths;

receiving and separating, by a beam splitting device, the incident light beam of a plurality of different wavelengths from the light source or the light conduction device, to form a plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam emitted in different emitting directions from the beam splitting device, wherein, each of the excitation light beams has a wavelength in a one-to-one correspondence with the plurality of different wavelengths of the incident light beam;

receiving, by a first dichroic mirror, the plurality of excitation light beams corresponding to the plurality of different wavelengths of the incident light beam in a one-to-one correspondence and emitted from the beam splitting device;

receiving, by an objective lens arranged between a sample to be detected and the first dichroic mirror, the plurality of excitation light beams transmitted by the first dichroic mirror, focusing, by the objective lens, the plurality of excitation light beams on a plurality

of different areas on the sample to excite a plurality of fluorescence in the plurality of different areas in one-to-one correspondence with the plurality of excitation light beams respectively, and transmitting, by the objective lens, the plurality of fluorescence to the first dichroic mirror; and

receiving, by a fluorescence guiding device, the plurality of fluorescence transmitted by the first dichroic mirror, and guiding, by the fluorescence guiding device, the plurality of fluorescence to a plurality of imaging devices corresponding to the plurality of fluorescence in a one-to-one correspondence, such that each fluorescence of the plurality of fluorescence is received and imaged by one of the plurality of imaging devices corresponding to the fluorescence to obtain fluorescence information corresponding to the fluorescence for detection.

43. The detecting method according to claim 42, wherein the beam splitting device is selected in such a manner that an included angle between emitting directions of excitation light beams of adjacent wavelengths among the plurality of excitation light beams emitted from the beam splitting device is not smaller than a threshold angle.

44. The detecting method according to claim 43, wherein the threshold angle is based on a ratio of a predetermined minimum spacing to a focal length of the objective lens, the predetermined minimum spacing indicating a minimum distance at which focusing spots formed on the sample by the plurality of excitation light beams need to be spaced apart from one another.

45. The detecting method according to claim 43 or claim 44, further comprising at least one of:

shaping, by a first beam shaping device located between the light source or the light conduction device and the beam splitting device, the incident light beam of a plurality of different wavelengths output from the light source or the light conduction device, and transmitting, by the first beam shaping device, shaped incident light beam to the beam splitting device; and

shaping, by a second beam shaping device located between the beam splitting device and the first dichroic mirror, the plurality of excitation light beams corresponding to the incident light beam of a plurality of different wavelengths in a one-to-one correspondence and emitted from the beam splitting device, and transmitting, by the second beam shaping

device, shaped plurality of excitation light beams to the first dichroic mirror.

46. The detecting method according to claim 45 when it depends on claim 44, wherein the second beam shaping device has an angular magnification, and in the case where the detecting method comprises shaping, by the second beam shaping device, the plurality of excitation light beams emitted from the beam splitting device, the threshold angle is equal to a product of the ratio of the predetermined minimum spacing to the focal length of the objective lens and a reciprocal of an absolute value of the angular magnification.

47. The detecting method according to any one of claims 42-44, wherein the beam splitting device comprises at least one dispersion prism.

48. The detecting method according to claim 47 when it depends on claim 43, wherein the at least one dispersion prism comprises a single dispersion prism positioned in such a manner that the incident light beam of a plurality of different wavelengths from the light source or the light conduction device is incident on a first refractive surface of the single dispersion prism and each of the plurality of excitation light beams then exits from a second refractive surface which is different from the first refractive surface, of the single dispersion prism.

49. The detecting method according to claim 48, wherein the incident light beam of a plurality of different wavelengths is incident on the first refractive surface of the single dispersion prism at a predetermined incident angle, the predetermined incident angle being selected in such a manner that a deviation angle between an incident direction of the incident light beam incident on the first refractive surface and an exit direction of the plurality of excitation light beams corresponding to the incident light beam exiting from the second refractive surface is minimized.

50. The detecting method according to claim 48, wherein the first refractive surface and the second refractive surface are adjacent surfaces of the single dispersion prism, the single dispersion prism has a vertex angle formed between the first refractive surface and the second refractive surface, and the single dispersion prism is selected in such a manner that a combination of the vertex angle of the single dispersion prism and a material selected to form the single dispersion prism enables the included angle to be not smaller than the threshold angle.

51. The detecting method according to claim 50, wherein the single dispersion prism

is a triangular prism.

52. The detecting method according to claim 47 when it depends on claim 43, wherein the at least one dispersion prism comprises a plurality of dispersion prisms that are sequentially arranged, each of the plurality of dispersion prisms having a vertex angle formed between a first refractive surface and a second refractive surface thereof that are adjacent and being positioned to receive each light incident thereon with the first refractive surface thereof and cause the light to exit from the second refractive surface thereof, wherein a combination of a number of the plurality of dispersion prisms and a vertex angle and a material of each of the plurality of dispersion prisms is selected in such a manner that the included angle is not smaller than the threshold angle.

53. The detecting method according to claim 52, wherein a first dispersion prism among the plurality of dispersion prisms that first receives the incident light beam of a plurality of different wavelengths from the light source or the light conduction device is positioned in such a manner that the incident light beam of a plurality of different wavelengths from the light source or the light conduction device is incident on a first refractive surface of the first dispersion prism and then exits from a second refractive surface of the first dispersion prism, and each of the plurality of dispersion prisms other than the first dispersion prism is positioned in such a manner that each of light exiting from an previous dispersion prism adjacent thereto is incident on a first refractive surface thereof and then exits from a second refractive surface thereof.

54. The detecting method according to any one of claims 42-44, wherein the beam splitting device comprises at least one grating.

55. The detecting method according to claim 42, wherein the fluorescence guiding device comprises a plurality of second dichroic mirrors that are sequentially arranged, the plurality of second dichroic mirrors comprising a last second dichroic mirror that is away from the first dichroic mirror and at least one preceding second dichroic mirror located between the last second dichroic mirror and the first dichroic mirror, the plurality of fluorescence received by the first dichroic mirror propagating sequentially through the plurality of second dichroic mirrors;

each preceding second dichroic mirror of the preceding second dichroic mirror(s) is positioned to guide one of at least one fluorescence incident thereon among the plurality of

fluorescence to the imaging device corresponding to the preceding second dichroic mirror, and to guide remaining fluorescence of the at least one fluorescence to a next second dichroic mirror adjacent to the preceding second dichroic mirror; and

the last second dichroic mirror is positioned to guide fluorescence incident thereon to the imaging device corresponding to the last second dichroic mirror.

56. The detecting method according to any one of claims 42-44 and 55, wherein the light source is an LED light source or a halogen light source, and the light conductive device is a single optical fiber.

57. The detecting method according to claim 56, wherein the single optical fiber is a coaxial coupled optical fiber.

58. The detecting method according to any one of claims 42-44 and 55, wherein the sample is a biological sample or a chemical sample.

59. The detecting method according to any one of claims 42 to 44 and 55, being used for gene detection.

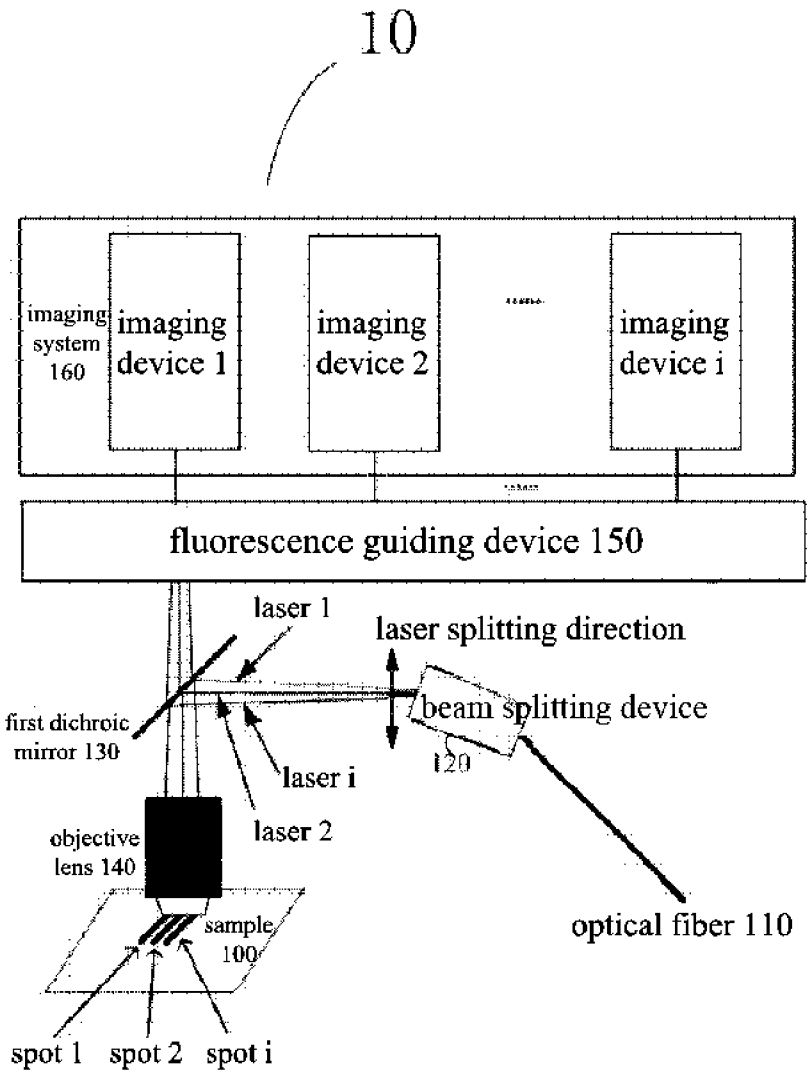

10
imaging system 160
imaging device 1
imaging device 2
imaging device i
fluorescence guiding device 150
laser 1
laser splitting direction
beam splitting device
120
first dichroic mirror 130
laser i
laser 2
objective lens 140
sample 100
optical fiber 110
spot 1
spot 2
spot i

FIG. 1a

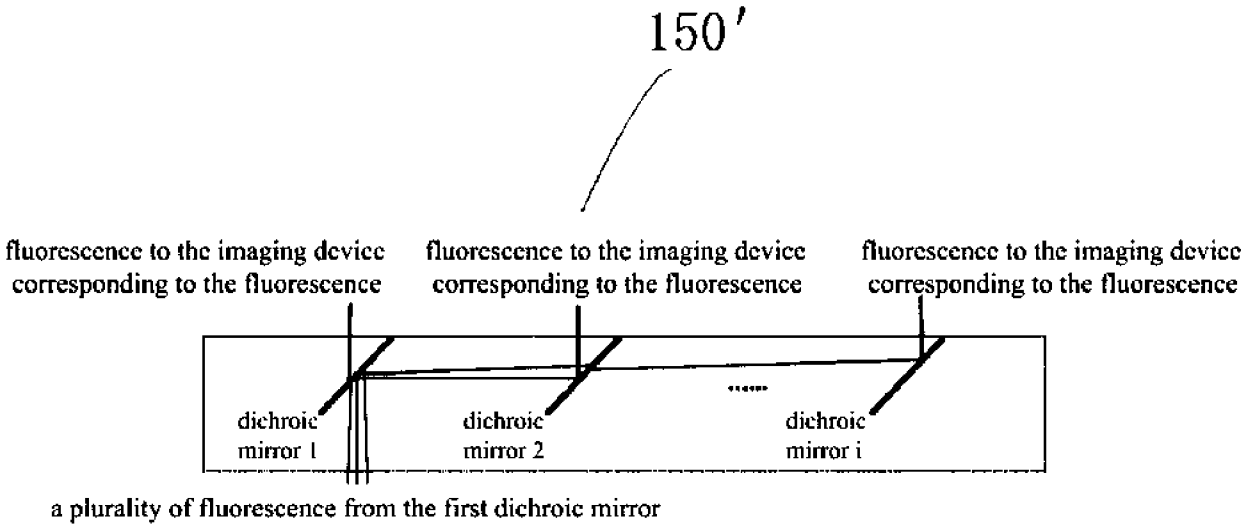

150'
fluorescence to the imaging device corresponding to the fluorescence
fluorescence to the imaging device corresponding to the fluorescence
fluorescence to the imaging device corresponding to the fluorescence
dichroic mirror 1
dichroic mirror 2
dichroic mirror i
a plurality of fluorescence from the first dichroic mirror

FIG. 1b

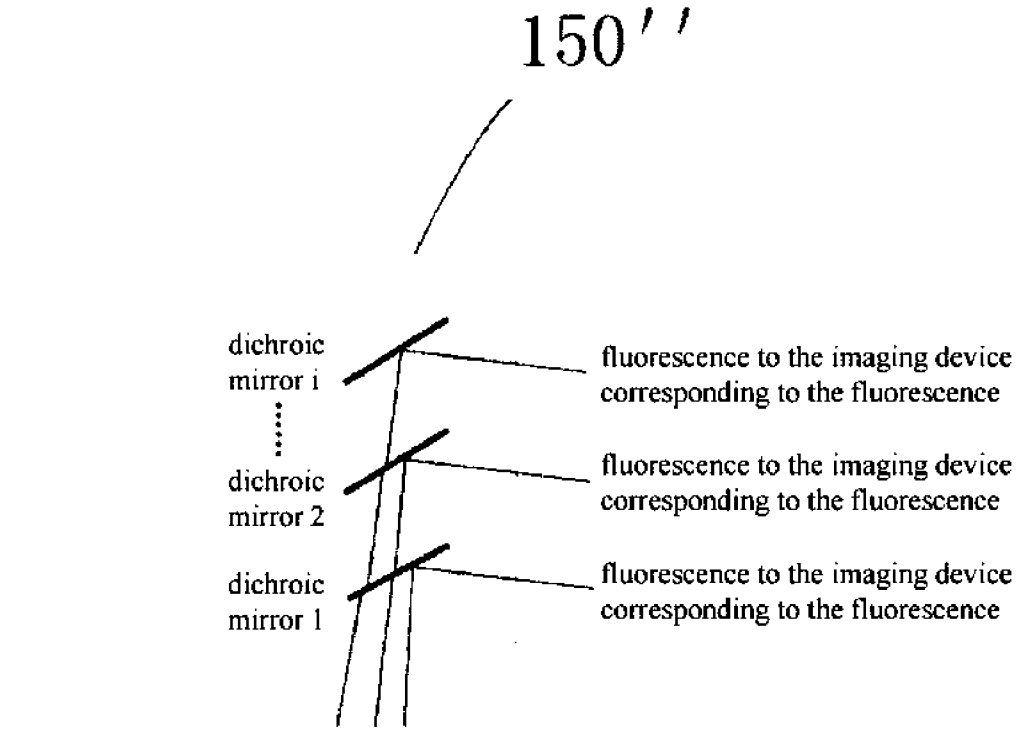

150''
dichroic mirror i
dichroic mirror 2
dichroic mirror 1
fluorescence to the imaging device corresponding to the fluorescence
fluorescence to the imaging device corresponding to the fluorescence
fluorescence to the imaging device corresponding to the fluorescence
a plurality of fluorescence from the first dichroic mirror

FIG. 1c

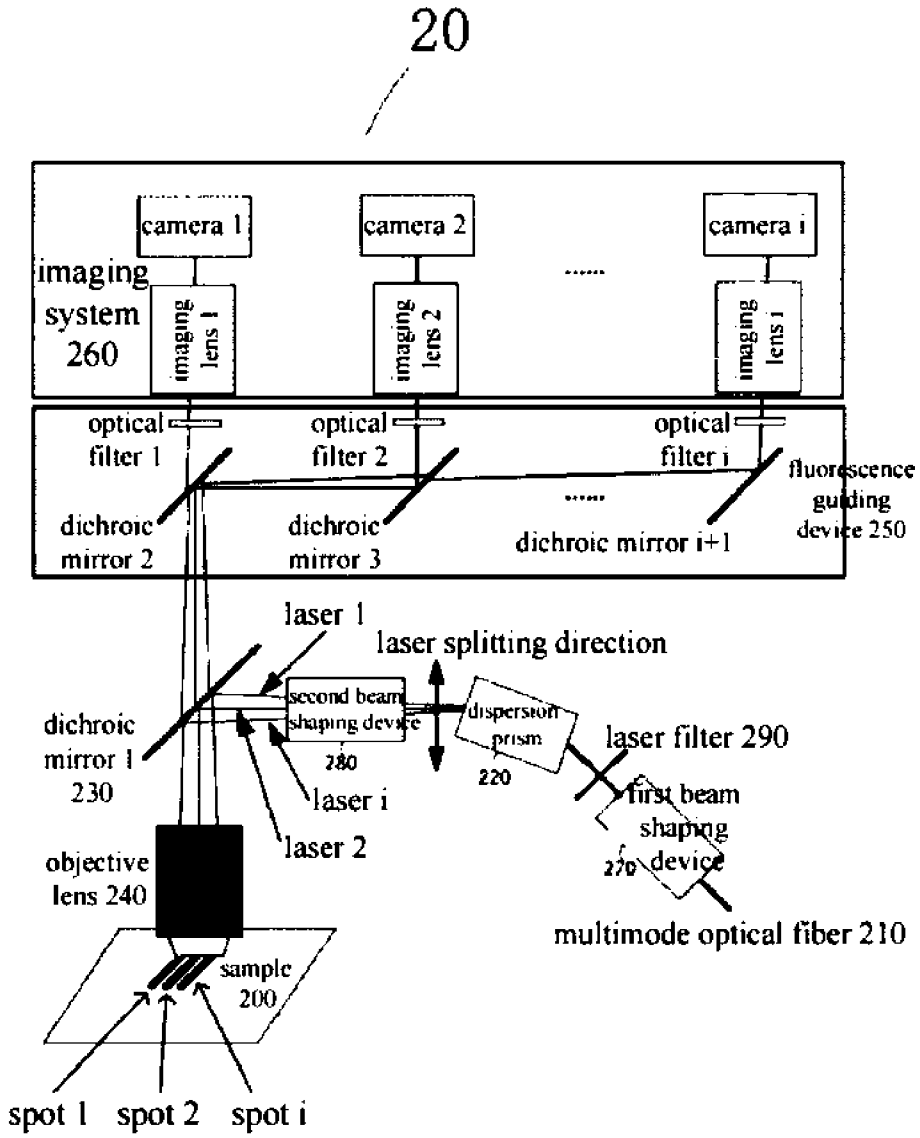

20
camera 1
camera 2
camera i
imaging system 260
imaging lens 1
imaging lens 2
imaging lens i
optical filter 1
optical filter 2
optical filter i
fluorescence guiding device 250
dichroic mirror 2
dichroic mirror 3
dichroic mirror i+1
laser 1
laser splitting direction
second beam shaping device 280
dispersion prism 220
laser filter 290
dichroic mirror 1 230
laser i
laser 2
first beam shaping device 270
objective lens 240
multimode optical fiber 210
sample 200
spot 1
spot 2
spot i

FIG. 2

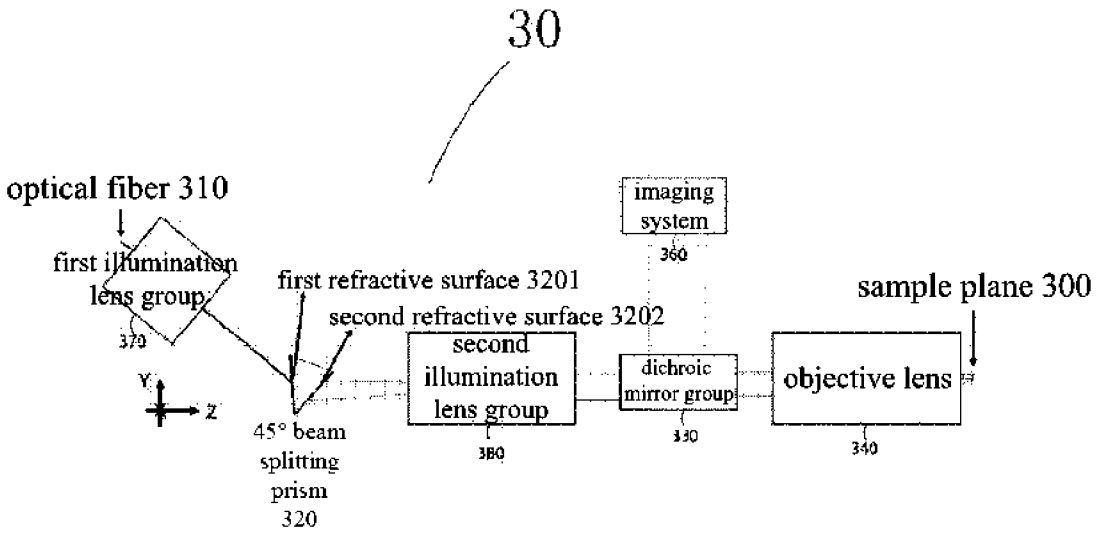

30
optical fiber 310
first illumination lens group 370
first refractive surface 3201
second refractive surface 3202
45° beam splitting prism 320
second illumination lens group 380
imaging system 360
dichroic mirror group 330
objective lens 340
sample plane 300
Y
Z

FIG. 3

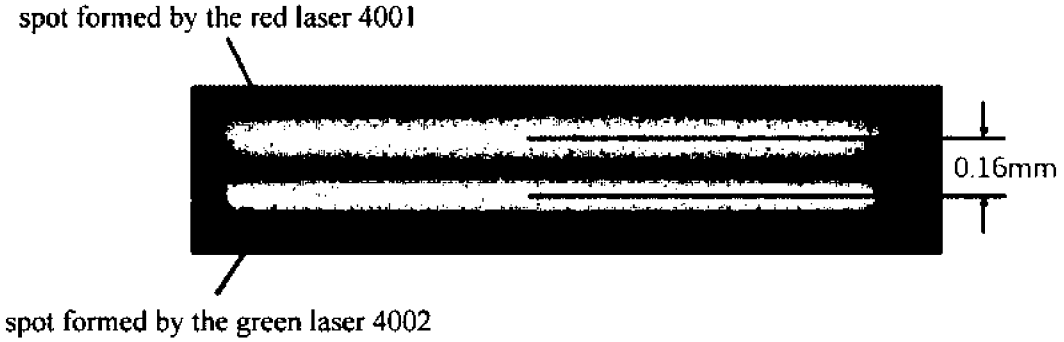

spot formed by the red laser 4001
0.16mm
spot formed by the green laser 4002

FIG. 4

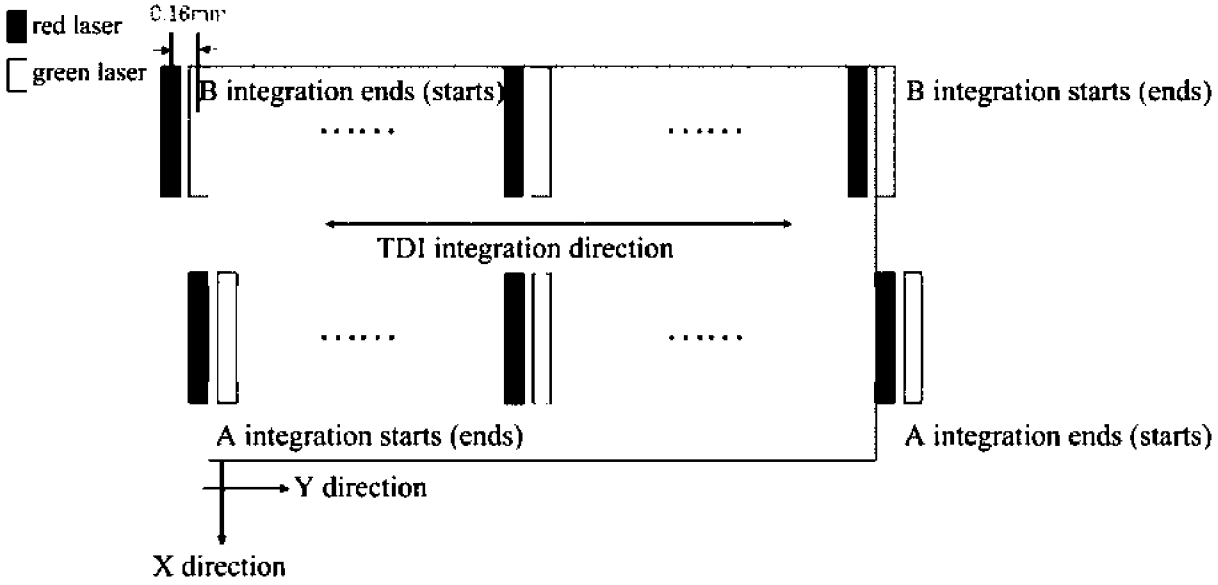

red laser
green laser
0.16mm
B integration ends (starts)
B integration starts (ends)
TDI integration direction
A integration starts (ends)
A integration ends (starts)
Y direction
X direction

FIG. 5

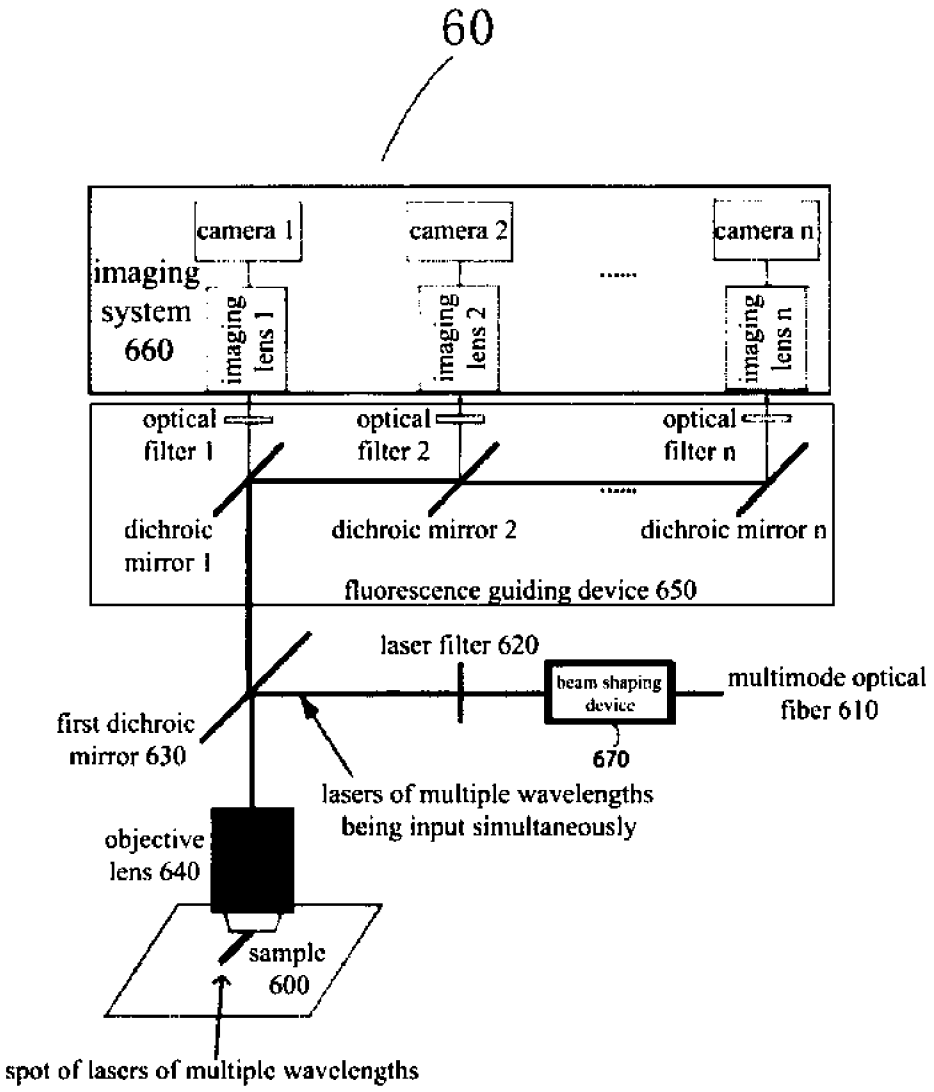

60
camera 1
camera 2
camera n
imaging system 660
imaging lens 1
imaging lens 2
imaging lens n
optical filter 1
optical filter 2
optical filter n
dichroic mirror 1
dichroic mirror 2
dichroic mirror n
fluorescence guiding device 650
laser filter 620
beam shaping device
multimode optical fiber 610
670
first dichroic mirror 630
lasers of multiple wavelengths being input simultaneously
objective lens 640
sample 600
spot of lasers of multiple wavelengths

FIG. 6

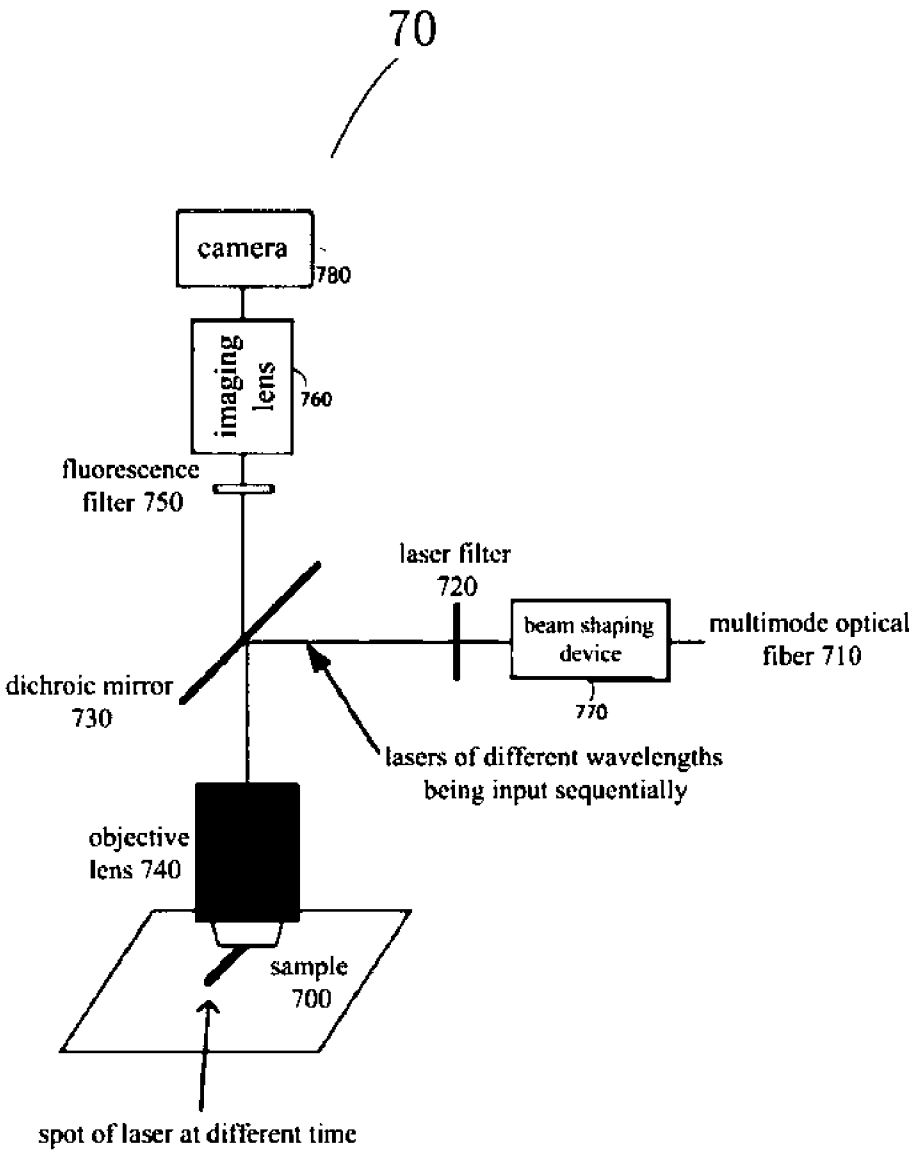

70
camera
780
imaging lens
760
fluorescence filter 750
laser filter 720
beam shaping device
770
multimode optical fiber 710
dichroic mirror 730
lasers of different wavelengths being input sequentially
objective lens 740
sample 700
spot of laser at different time

FIG. 7

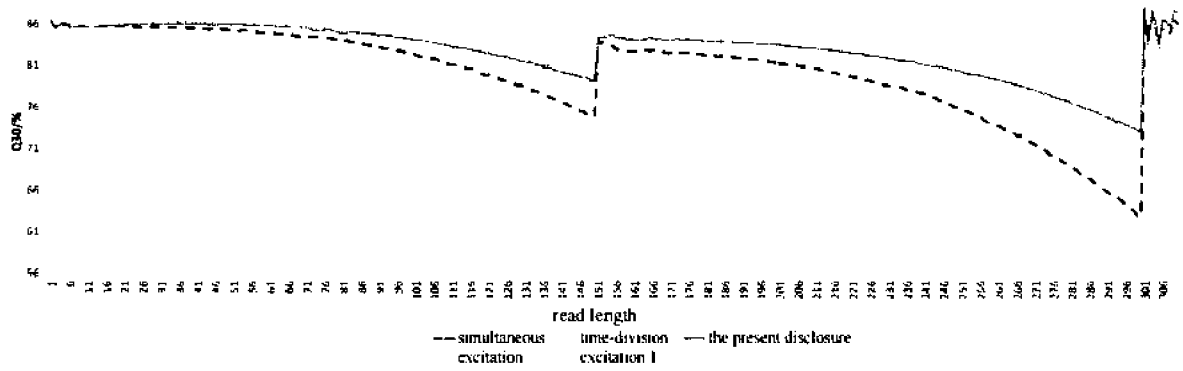

Q30/%
read length
simultaneous excitation
time-division excitation I
the present disclosure

FIG. 8a

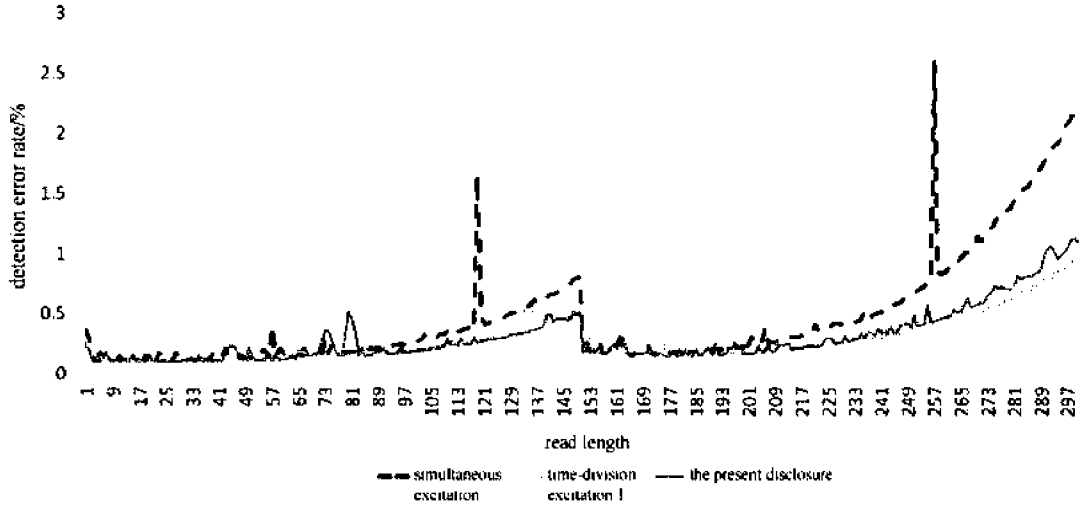

detection error rate/%
read length
simultaneous excitation
time-division excitation I
the present disclosure

FIG. 8b

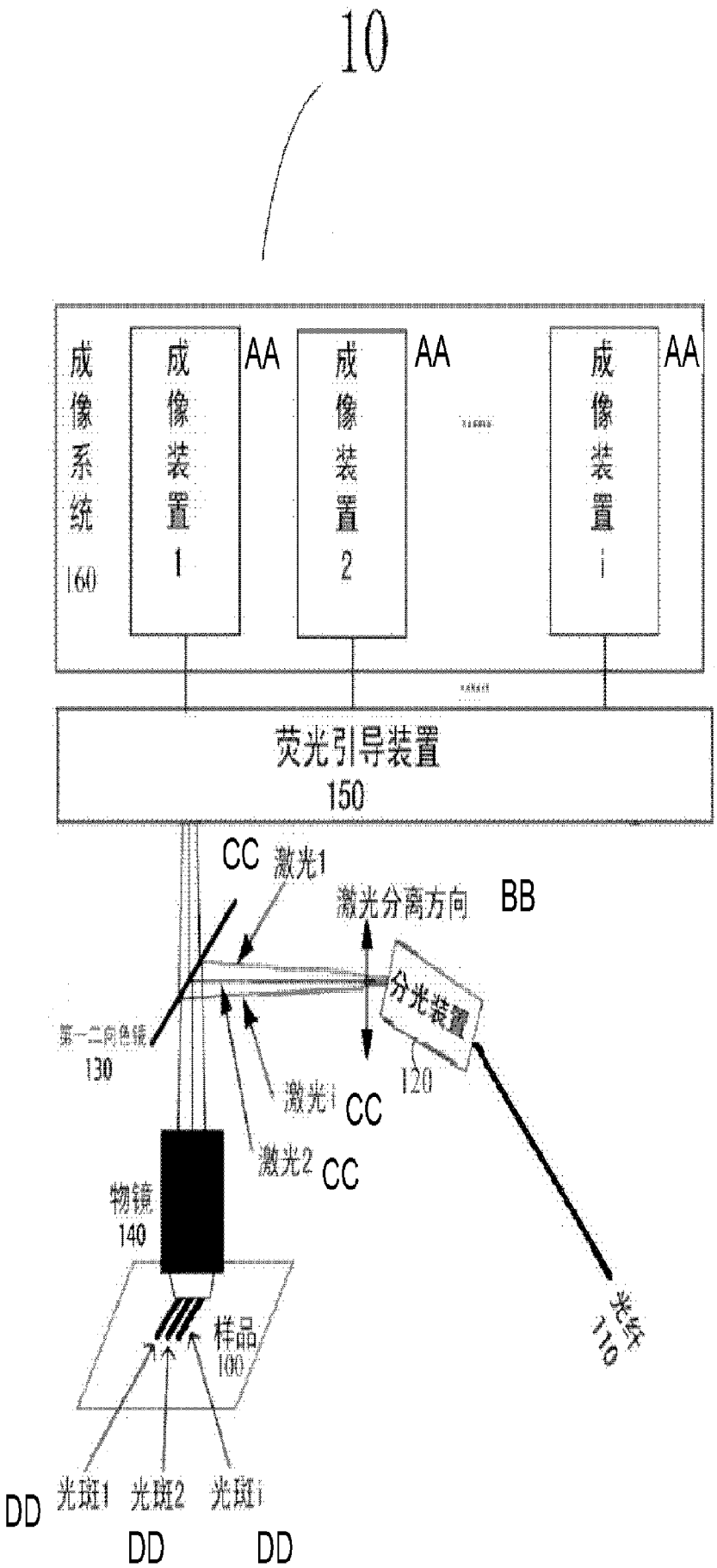


图 1a

100	Sample
110	Optical fiber
120	Beam splitting apparatus
130	First dichroscope
140	Objective lens
150	Fluorescence guide apparatus
160	Imaging system
AA	Imaging apparatus
BB	Laser separation direction
CC	Laser
DD	Light spot