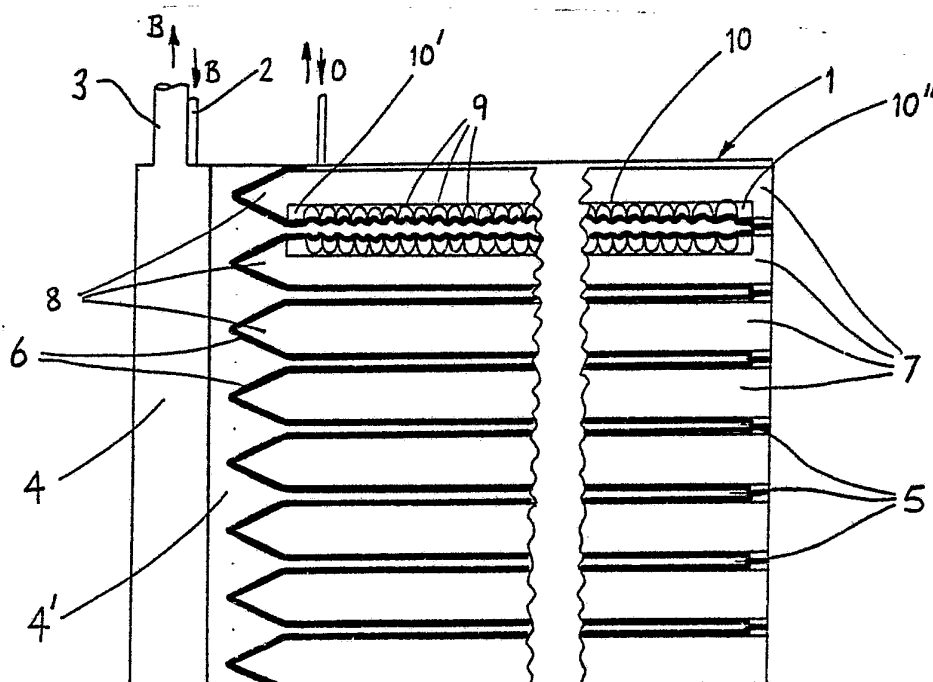




INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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<p> (21) International Application Number: PCT/GB83/00324 (22) International Filing Date: 7 December 1983 (07.12.83) (31) Priority Application Number: 8234892 (32) Priority Date: 7 December 1982 (07.12.82) (33) Priority Country: GB (71)(72) Applicant and Inventor: BELLHOUSE, Brian, John [GB/GB]; The Lodge, North Street, Islip, Oxfordshire OX5 2SQ (GB). (74) Agent: GILL JENNINGS & EVERY; 53 to 64, Chan- cery Lane, London WC2A 1HN (GB). (81) Designated States: AU, BR, DK, JP, NO, US. Published <i>With international search report.</i> <i>With amended claims and statement.</i> </p>		

(54) Title: TRANSFER MEMBRANE APPARATUS**(57) Abstract**

A membrane assembly, for use in mass or heat transfer or filter apparatus, comprises a pair of generally parallel plates (7) spaced apart with a profiled surface of one plate facing a similarly profiled surface of the other plate. A pair of sheets of transfer membrane material (6) are positioned closely spaced face to face between the plates with each sheet supported by and partially nesting in the profiled surface of the adjacent plate. The two membrane sheets thus provide a conduit (5) for one fluid. Between each sheet and the adjacent plate is formed a conduit for the second fluid. In use each sheet presents in its surface facing the other sheet a regular array of close packed depressions (14) which partially nest in corresponding depressions (9) in the respective plates (7).

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TRANSFER MEMBRANE APPARATUS

5 The invention relates to apparatus for effecting
transfer of heat or mass between two fluids, of which
at least one is usually a liquid, through a transfer
membrane. Such apparatus is used in blood
oxygenators and dialysers, in which case one fluid is
blood and the other is oxygen or dialysate. In
10 practice the efficiency of the transfer across the
membrane is limited by the extent to which the total
volume of fluid can be brought into close proximity
with the membrane.

GB-A-1,442,754 describes an apparatus wherein
15 the membrane surface exposed to the fluid in one of
the conduits is provided with a regularly repeating
array of hollows, and there is superimposed on the
mean flow of fluid through the conduit a pulsatile
component which promotes vortex mixing of the fluid
20 in the hollows.

It has been proposed to provide the conduit, in
which the vortex mixing occurs, between two closely
spaced generally planar sheets of transfer membrane
material, in at least one of which the hollows are
25 formed. The hollows proposed were then furrows
extending transversely to the pulsatile component in
the fluid flow. The furrows may be preformed in the
membrane or produced by initial stretching of the
membrane by fluid in the conduit whilst the membrane
30 is supported externally against a profiled support
plate. In that case a conduit for the second fluid
is provided between the membrane and the support
plate. There are advantages however in providing the
conduits, in which the vortex mixing is promoted, in
35 the form of axisymmetric tubular conduits having a
series of larger cross-sectional bulbous portions
connected by smaller cross-sectional neck portions.

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However, such tubular conduits are difficult to mount in the apparatus. GB-A-2,042,926 discloses a technique for making an integral array of tubular conduits by sealing together two sheets, of which at least one is transfer membrane material, along a series of sinuous lines extending generally in the same direction alongside one another, with the undulations of adjacent lines out of phase with one another. This provides a generally planar compact nesting array of conduits. Each bulbous portion of each conduit is positioned between neck portions of adjacent conduits. However problems arise in sealing, e.g. by means of heat, the delicate transfer membrane material. Also, narrow crevices tend to be formed along the sides of the conduit adjacent to the seal lines and these provide possible locations for blood to collect and clot.

In accordance with the present invention, a membrane assembly for use in mass or heat transfer or filter apparatus, comprises a pair of generally parallel plates spaced apart with a profiled surface of one plate facing a similarly profiled surface of the other plate; and a pair of sheets of transfer membrane material closely spaced face to face between the plates with each sheet supported by and partially nesting in the profiled surface of the adjacent plate, to provide between the membranes a conduit for one fluid and, between each sheet and the adjacent plate a conduit for the second fluid; whereby in use each sheet presents in its surface facing the other sheet a regular array of close packed depressions. Preferably, each of the depressions faces a similar depression in the other sheet.

Surprisingly this geometry provides extremely good fluid dynamics in the conduit between the two membrane sheets. Specifically, since the membrane sheets are spaced, at least slightly, throughout the



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majority of their areas, hydraulic resistance is low, and yet adequate vortex mixing can be promoted in the depressions with a small pulsatile component of flow superimposed upon the mean flow of fluid through the conduit. Even compared with apparatus in which the liquid flow rate is already turbulent, ie. with Reynold's numbers of say greater than 15,000, with the apparatus of the invention there is an effective trebling of the mass transfer rate. When the fluid is blood, the positive spacing of the membrane sheets, substantially throughout their whole area, minimizes the existence of any places where stagnation and clotting of blood may occur.

Although the apparatus is primarily designed for mass or heat transfer, it could also be used in filtration apparatus, for example for filtering off small blood cells and plasma, with the liquid supplied under greater pressure than in conventional transfer applications. The invention overcomes the problems associated with concentration polarization which in conventional filtration apparatus for say blood, prevents the small cells from passing through the filter. In such apparatus a single membrane sheet may be provided on the inside of a tubular support which is profiled on its inside, the depressions in the membrane sheet lying in similar depressions which form the profiling in the support.

In a preferred construction, the depressions in each membrane sheet are close packed by being provided in rows extending side by side to one another along the direction of mean flow through the conduit, the depressions in adjacent rows being longitudinally offset halfway between adjacent depressions in the adjacent rows so that lateral nesting of adjacent rows occurs. This arrangement will be seen to be analogous to that disclosed in GB-A-2,042,926 which suggests that the profiled



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surfaces of the support plates may be provided with sinuous ribs extending side by side along the conduit with the undulations in adjacent ribs out of phase with one another. However, the production of support plates with such sinuous ribs would be expensive by moulding or otherwise.

I find that in fact it is sufficient if the profiled surfaces of the plates are formed by drilling or otherwise providing part-spherical depressions in alignment with the depressions in the membrane sheet. In order to prevent the partial nesting of each membrane sheet in the part spherical depression in the respective support plate from sealing one support plate depression from the next, and hence the passage of the second fluid through the second conduit between the membrane sheet and adjacent plate, the depressions in the plate are preferably interconnected by shallow grooves. This enables free passage of the second fluid and, if the depressions are arranged in longitudinal rows, the grooves preferably interconnect one depression to the next along the respective row. This enables the second fluid to be passed in countercurrent to the first fluid and also has the advantage that the membrane sheet can partially nest in the groove and provide a less restricted passage for the one fluid through the one conduit between the membrane sheets. Transversely extending grooves may also be provide across the rows to prevent stagnation along a whole row resulting from blockage of a single depression in that row.

The depressions in each membrane may be formed by pre-embossing the membrane sheets, using heat and pressure, if for example they are made of a thermoplastic material such as polypropylene. Alternatively, the sheets may be stretched and shaped in situ by being partially forced into the profiling



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of the support plates, utilizing a hot liquid under pressure when the apparatus is first assembled.

5 The construction described is particularly useful for a blood oxygenator, in which blood will be the one liquid passed with a pulsatile flow through the one conduit between the membrane sheets, and oxygen will be the second fluid passed through the two second conduits in countercurrent to the blood. Experiments have shown that, when the blood is
10 perfused with an ordinary roller pump, both oxygen and carbon dioxide are transferred at about 200 $\text{ml} \cdot \text{min}^{-1} \cdot \text{m}^{-2}$. When reversing pulsatile flow, i.e. flow in which the superimposed pulsatile component is sufficient to cause once each cycle a slight reversal
15 in the flow of blood, in the direction opposite to the mean flow, gas transfer increased up to 450 $\text{ml} \cdot \text{min}^{-1} \cdot \text{m}^{-2}$. This is a higher gas transfer than I have obtained with any other apparatus of the kind described. The gas transfer rates referred to above
20 were both obtained with a minimum membrane sheet separation of 0.5 mm.

One example of apparatus incorporating a membrane assembly according to the present invention will now be described with reference to the
25 accompanying drawings, in which:

Figure 1 shows a side sectional elevation of the apparatus;

Figure 2A shows a plan view of a membrane of the assembly according to the invention;

30 Figure 2B shows a plan view of a plate used in the apparatus;

Figure 3 shows, in plan, a part of the membrane in greater detail;

35 Figure 4 shows, in plan, part of a support plate for the membrane in greater detail; and

Figure 5 is a detailed sectional view of a pair of plates of the apparatus shown in Figure 1 with the



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membrane between.

The apparatus shown in Figure 1 forms part of an artificial lung and has a rectangular housing 1 with an inlet 2 and outlet 3 through which blood is fed to the housing. Manifolds, separated by a wall 4 with a rubber sealing portion 4', enable blood to be supplied to a stack of U-shaped conduits 5 formed by a polypropylene microporous membrane 6 which is disposed in a sinuous folded path around the front of and between a plurality of stacked, spaced apart, plates 7. Each of the plates 7 is injection moulded from polycarbonate and has a tapered front end 8 which provides faired inlet and outlet portions to the U-shaped conduits 5 formed between the plates 7 by the membrane 6.

As shown in greater detail in Figures 4 and 5, each of the plates 7 is formed with a plurality of part-spherical depressions 9 extending in rows from a point just adjacent the front of the plate to a point well spaced from the rear of the plate. As shown in Figure 2B and Figure 4 the depressions 9 in adjacent rows are closely packed, so that adjacent depressions 9 are substantially equi-distantly spaced apart, by offsetting adjacent rows by half the spacing between the centres of adjacent depressions in each row. Connecting the depressions along each respective row is a groove 10 formed to the same depth as the depressions 9. For simplicity, the depressions 9 are shown only in the top pair of plates in Figure 1 and, at that, only diagrammatically. Figures 4 and 5 illustrate the formation of the depressions and grooves more accurately as they are drawn to a larger scale.

To feed oxygen to the grooves 10 and depressions 9, manifold apertures 20 are formed in the front side edges of each plate as shown in Figure 2B. Grooves 10' feeding the oxygen from the apertures to the



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front ends of the slots 10 and grooves 10" feeding the oxygen across the rear of the plate between the two sides of the U-shaped path.

5 The membrane 6 is laid-up in a sinuous path between the plates 7 as shown in Figure 1 and each conduit 5 is formed in a U-shape as shown more particularly by Figure 2 which illustrates, in plan, one side of one of the conduits formed by the membrane 6. The membrane 6 is held between the
10 plates by rubber gaskets which press against the two membrane portions and squeeze them together to form a seal. At either end of the side portion of the conduit-forming membrane sheet 6 are fold lines 11,12 about which the membrane is folded at the front of
15 the stack of plates and at the back respectively.

The arrows B in Figure 2 illustrate the flow path of blood from and to the inlet and outlet manifolds within the conduit formed by the two superimposed areas of the membrane 6 which lie between a
20 respective pair of the plates 7. In longitudinally extending areas 13 the membrane is dimpled outwardly of the conduit, the dimples 14 being provided, as with the depressions in the plates 7, in longitudinally extending rows, adjacent rows being
25 offset by half the distance between the centres of the dimples. The dimples 14 are preferably formed in the membrane prior to it being folded and stacked with the plates 7, but it is envisaged that when the membrane is formed of thermoplastic materials, the
30 dimples could be formed in situ from an essentially planar membrane, by passing, for example hot water, under pressure through the conduits after initial assembly so as to stretch the membrane into the depressions 9 to form the dimples 14.

35 Longitudinal ribs 15 separate the adjacent longitudinal dimpled sections 13 and in the centre of the membrane a wider rib portion 16 is provided, the

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two sheet portions of the membrane 6 which form each side of a conduit being sealed to one another along this portion 16 so as to define the generally U-shaped path for the blood. Each of the plates 7 has a corresponding rib portion (not shown) of substantially the same length as the portion 16, the opposed rib portions on adjacent plates squeezing the membrane between them so as to produce the seal along the portion 16. Side portions 17 on each side of the conduit are likewise sealed between corresponding side portions of adjacent plates 7 to seal the edges of the conduit.

As indicated by the arrows 0 in Figure 2, the flow of oxygen through the artificial lung also follows a U-shaped path around each conduit 5, the oxygen being fed from the apertures 20, through the grooves 10', under the dimpled portions 14, through the depressions 9 and the grooves 10, and across the undimpled portion 18 of the conduit through the grooves 10" and then back down a similar path on the other side. Oxygen is fed to the apertures through suitable ducts (not shown).

In the particular example shown the dimples in the membrane sheet 6 and the depressions 9 are arranged in alignment with one another so that, as shown in Figure 5, the dimples 14 extend partly into the depressions 9. Each of the dimples and depressions has a diameter of substantially 1.5 mm., the dimples having a depth of 0.5 mm. and the depressions a depth of 1 mm., the grooves 10 having a width of 0.5 mm. and a depth, the same as the depressions, i.e. 1 mm. The portions of the plates 7 which have the depressions formed in them are spaced apart a distance of 0.5 mm.

In use, blood is pumped through the artificial lung preferably with a pulsatile flow, for example, by means of a pair of rolling-diaphragm piston pumps



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which may be located in the respective manifolds and which are operated in anti-phase to produce oscillating blood flow inside the lung. Blood will thus flow in a plurality of U-shaped paths through the conduits 5 formed by the folded membrane 6. The blood flows with a mean flow velocity through the conduits 5, but the superimposed reciprocatory component causes the blood alternately to accelerate and decelerate and this sets up eddies or vortices in the dimples 14 to promote intimate mixing of the blood and contact between the blood and the transfer membrane. At the same time oxygen is pumped in a steady stream through the housing in countercurrent to the flow of blood, also in U-shaped paths between the conduits 5 formed by the membrane and the plates 7. The countercurrent flow of oxygen produces good transfer through the membrane walls of the conduits.

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CLAIMS

1. A membrane assembly, for use in mass or heat transfer or filter apparatus, the assembly comprising
5 a pair of generally parallel plates (7) spaced apart with a profiled surface of one plate facing a similarly profiled surface of the other plate; and a pair of sheets of transfer membrane material (6) closely spaced face to face between the plates with
10 each sheet supported by and partially nesting in the profiled surface of the adjacent plate, to provide between the membranes a conduit (5) for one fluid and, between each sheet and the adjacent plate a conduit for the second fluid; whereby in use each
15 sheet presents in its surface facing the other sheet a regular array of close packed depressions (14).

2. An assembly according to claim 1, wherein each of the depressions (14) faces a similar depression in
20 the other sheet.

3. An assembly according to claim 1 or claim 2, wherein the depressions (14) in each sheet are provided in rows extending side by side to one
25 another along the direction of mean flow through the conduit (5), the depressions (14) in adjacent rows being longitudinally offset halfway between adjacent depressions in the adjacent rows so that lateral nesting of adjacent rows occurs.

30 4. An assembly according to any of claims 1 to 3, wherein the profiled surfaces of the plates (7) are provided by circular depressions (9) in alignment with the depressions in the membrane sheet (6).

35 5. An assembly according to claim 4, wherein the circular depressions (9) in the plates (7) are



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part-spherical.

5 6. An assembly according to claim 4 or claim 5, wherein the depressions (9) in the plates (7) are interconnected by grooves (10).

10 7. An assembly according to claim 6, wherein the depressions (9) in the plates (7) are arranged in longitudinal rows along the direction of mean flow along the assembly, the grooves (10) interconnecting one depression to the next along the respective row.

15 8. A method of making an assembly according to any of claims 1 to 7, wherein after assembly of a pair of planar membrane sheets (6) with the plates (7), fluid under pressure is supplied between the sheets at least partially forcing the sheets into the depressions (9) in the respective plates to permanently deform the sheets to form the depressions (14) therein.

25 9. A method according to claim 8, wherein the sheets are formed of a thermoplastic material and the fluid is a hot liquid.

30 10. A microporous transfer membrane for use in mass or heat transfer or filter apparatus, the membrane having a surface with a regular array of close packed depressions (14).

35 11. A membrane filter assembly having a membrane according to claim 10, the membrane being supported internally of a similarly profiled and apertured tubular support member.



AMENDED CLAIMS

[received by the International Bureau on 12 June 1984 (12.06.84);
original claims 1 to 11 replaced by amended claims 1 to 7]

1. A membrane assembly, for use in mass or heat transfer apparatus, the assembly comprising a pair of
5 generally parallel plates (7) spaced apart with a profiled surface of one plate facing a similarly profiled surface of the other plate; and a pair of sheets of transfer membrane material (6) closely spaced face to face between the plates with each
10 sheet supported by and partially nesting in the profiled surface of the adjacent plate, to provide between the membranes a first conduit (5) for a first fluid and, between each sheet and the adjacent plate a second conduit for a second fluid; each sheet
15 presenting in its surface facing the other sheet a regular array of close packed permanent dimple-like depressions (14), each facing and substantially aligned with a similar depression in the other sheet, whereby, in use, when the one fluid is passed through
20 the first conduit (5) with a pulsatile flow, vortex mixing occurs in the depressions.

2. An assembly according to claim 1, wherein the depressions (14) in each sheet are provided in rows
25 extending side by side to one another along the direction of mean flow through the conduit (5), the depressions (14) in adjacent rows being longitudinally offset halfway between adjacent depressions in the adjacent rows so that lateral
30 nesting of adjacent rows occurs.

3. An assembly according to claims 1 or claim 2, wherein the profiled surfaces of the plates (7) are provided by circular depressions (9) in alignment
35 with the depressions in the membrane sheet (6).



4. An assembly according to claim 3, wherein the circular depressions (9) in the plates (7) are part-spherical.
- 5 5. An assembly according to claim 3 or claim 4, wherein the depressions (9) in the plates (7) are interconnected by grooves (10).
- 10 6. An assembly according to claim 5, wherein the depressions (9) in the plates (7) are arranged in longitudinal rows along the direction of mean flow along the assembly, the grooves (10) interconnecting one depression to the next along the respective row.
- 15 7. Apparatus for mass or heat transfer between first and second fluids, the apparatus comprising a membrane assembly according to any one of the preceding claims, connected to both a first pumping means for pumping the first fluid through the first
- 20 conduit with a pulsatile flow, and a second pumping means for pumping the second fluid through the second conduit.



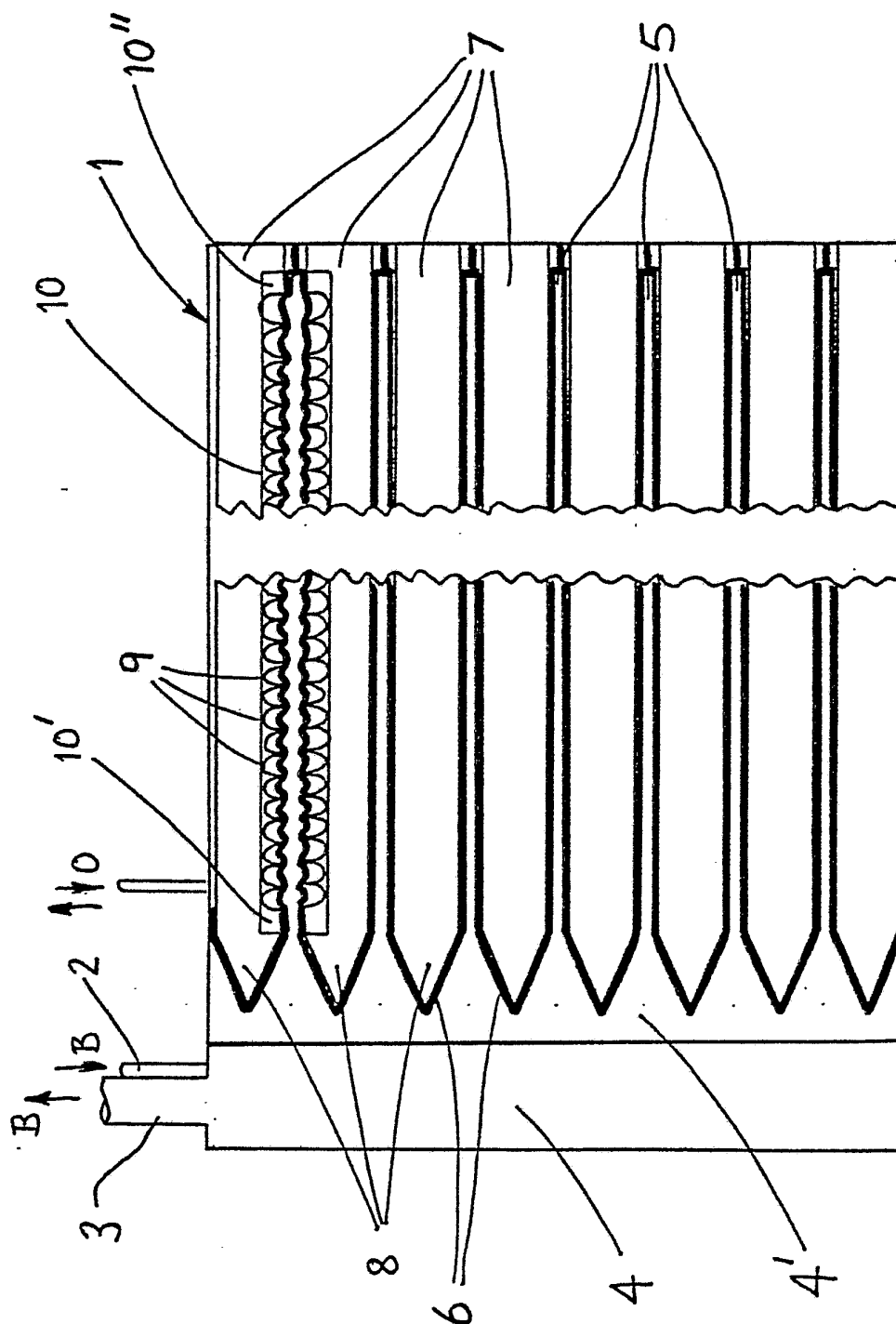
STATEMENT UNDER ARTICLE 19

Claim 1 of the new set of seven claims, on which all the other claims are now dependent, is restricted to the depressions being permanent and dimple-like, and to the depressions in one membrane sheet being substantially aligned with respect to similar depressions in the other membrane sheets so that when the one fluid is passed through the first conduit with a pulsatile flow, vortex mixing occurs in the depressions. This claim distinguishes clearly from all the cited art.



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Fig1.



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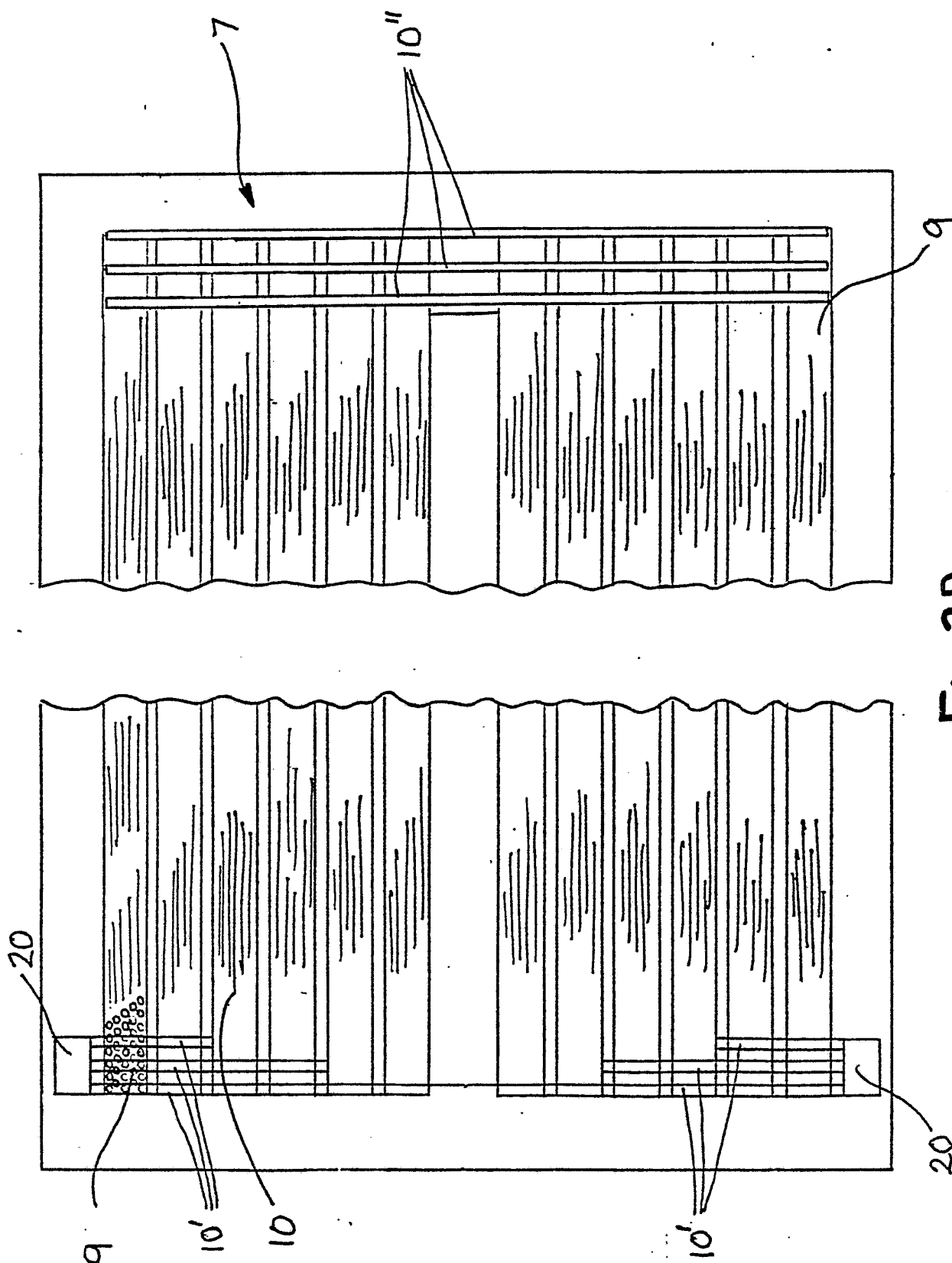


Fig 2B

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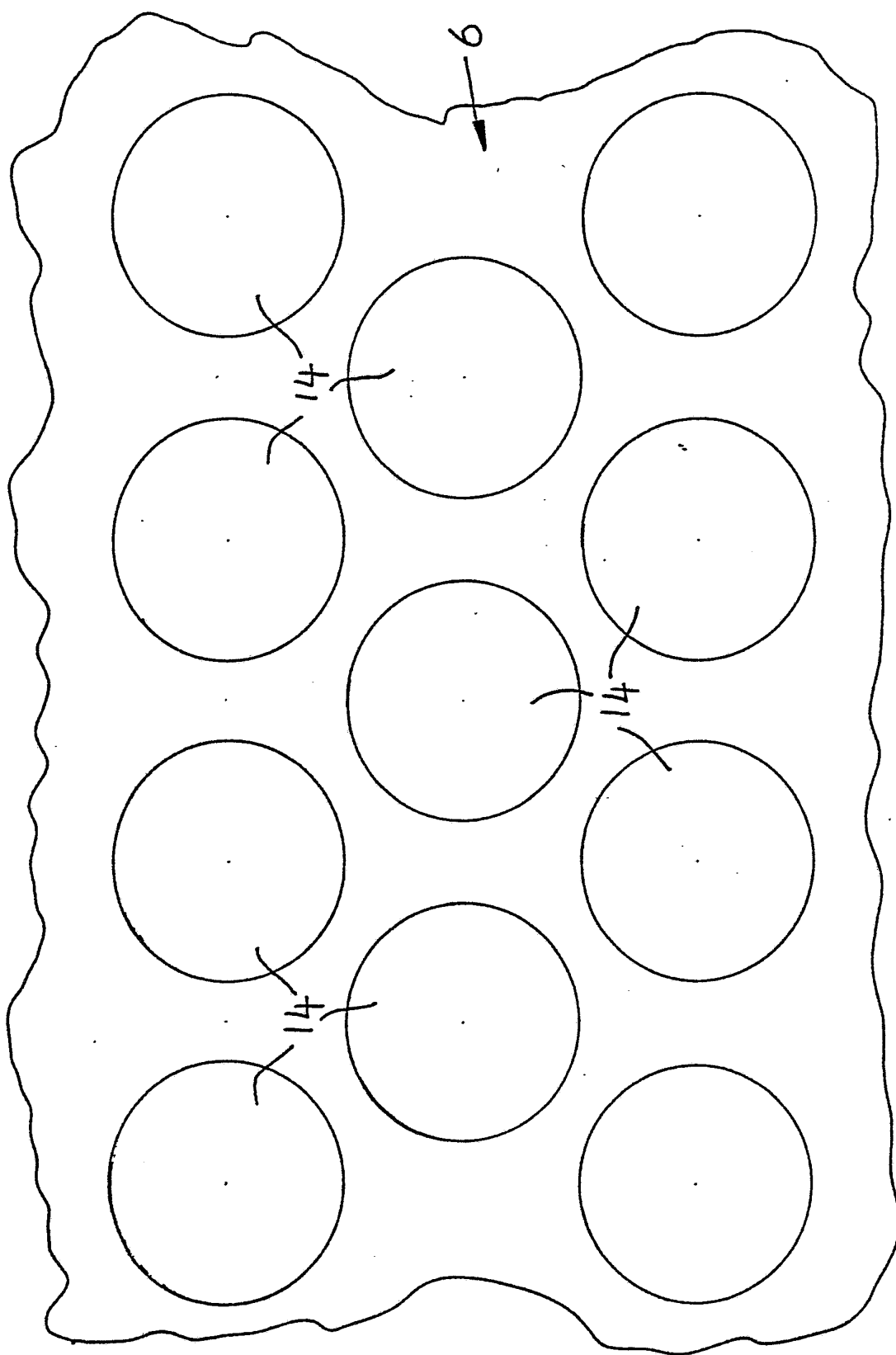


Fig 3

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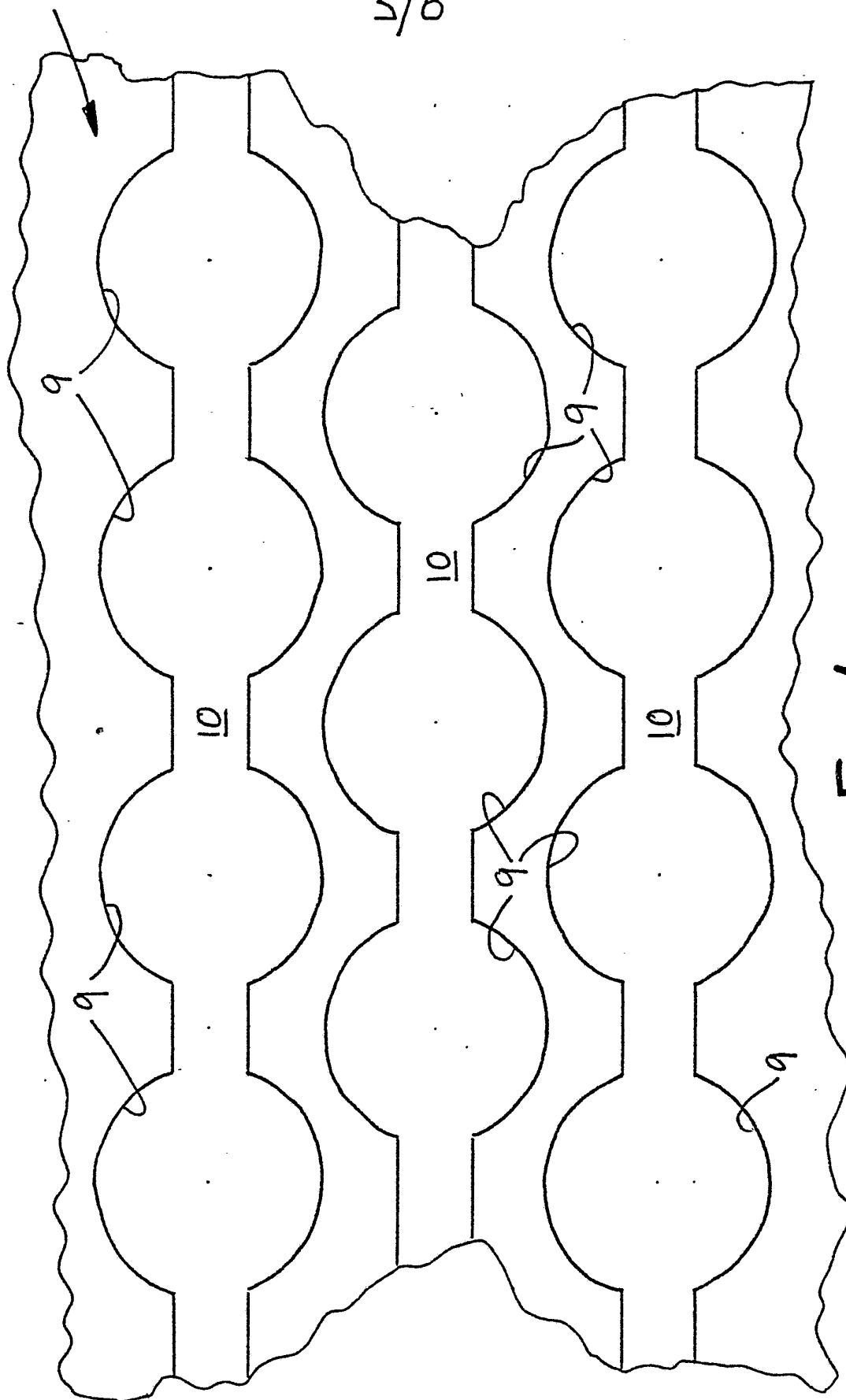
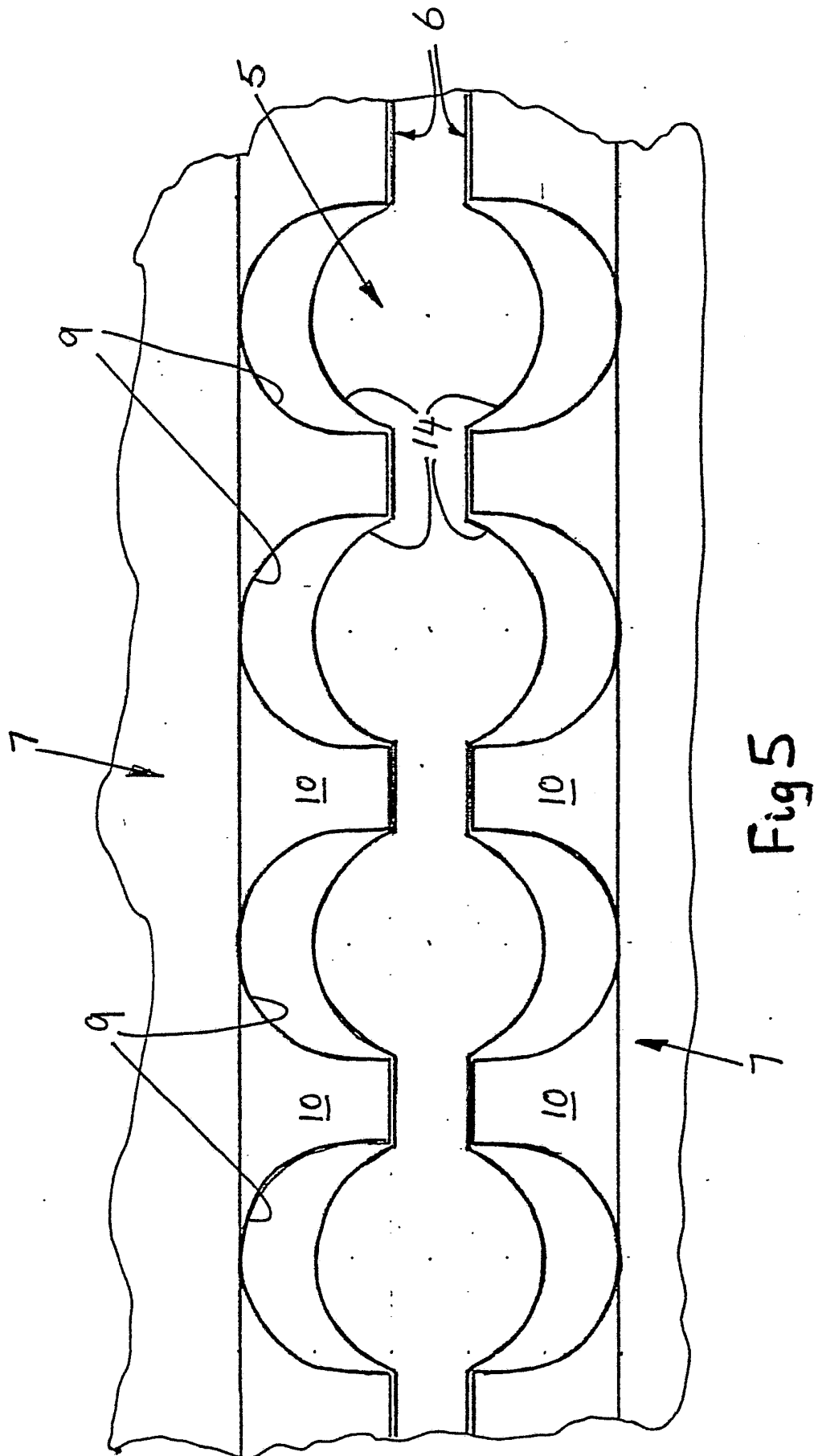


Fig 4

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INTERNATIONAL SEARCH REPORT

International Application No PCT/GB 83/00324

I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all) ³		
According to International Patent Classification (IPC) or to both National Classification and IPC		
IPC ³ : A 61 M 1/03; B 01 D 13/00		
II. FIELDS SEARCHED		
Minimum Documentation Searched ⁴		
Classification System	Classification Symbols	
IPC ³	A 61 M; B 01 D	
Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched ⁵		
III. DOCUMENTS CONSIDERED TO BE RELEVANT ¹⁴		
Category ⁶	Citation of Document, ¹⁶ with indication, where appropriate, of the relevant passages ¹⁷	Relevant to Claim No. ¹⁸
X	DE, A, 2810949 (SIGDELL) 11 October 1979 see the complete document, in particular figures 5,7,8,15; page 7, lines 27-33	1,3,4
Y	--	2,6-8
Y	WO, A, 80/01042 (BELLHOUSE) 29 May 1980 see the complete document, in particular figure 5; page 1, lines 1-4; page 9, line 29 - page 10, line 3	2,8
X	--	10
A	--	9
X	US, A, 3724673 (GENERAL ELECTRIC) 3 April 1973 see the complete document, in particular figures 4,5; claims 1-3	10
X	FR, A, 2368284 (NATIONAL RESEARCH) 19 May 1978 see figures 2,3	1,2
A	FR, A, 2370497 (EXTRACORPOREAL) 9 June 1978 see figures 2-5	5 ./.
<p>* Special categories of cited documents: ¹⁵</p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"&" document member of the same patent family</p>		
IV. CERTIFICATION		
Date of the Actual Completion of the International Search ¹	Date of Mailing of this International Search Report ²	
9th March 1984	18 AVR. 1984	
International Searching Authority ¹	Signature of Authorized Officer ²⁰	
EUROPEAN PATENT OFFICE	G.L.M. Kruidenberg	

III. DOCUMENTS CONSIDERED TO BE RELEVANT (CONTINUED FROM THE SECOND SHEET)		
Category *	Citation of Document, ¹⁶ with indication, where appropriate, of the relevant passages ¹⁷	Relevant to Claim No ¹⁸
X	DE, A, 2842118 (KATO) 5 April 1979 see figures 1-6, 14, 15A-15D; page 12, lines 10-23; page 15, lines 15-17	10
Y	--	6, 7
X	US, A, 4075091 (NATIONAL RESEARCH) 21 February 1978 see figures 4, 5 -----	10, 11

ANNEX TO THE INTERNATIONAL SEARCH REPORT ON

INTERNATIONAL APPLICATION NO. PCT/GB 83/00324 (SA 6211)

This Annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report. The members are as contained in the European Patent Office EDP file on 06/04/84

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Patent document cited in search report	Publication date	Patent family member(s)	Publication date
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INTERNATIONAL APPLICATION NO.

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