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WO-A-00/35450
WO-A-00/59479
WO-A-99/03471

DESCRIPTION

BACKGROUND OF THE INVENTION

[0001] Methylphenidate Hydrochloride, a scheduled II controlled substance, is currently marketed as a mild central nervous system (CNS) stimulant and the drug of choice for treatment of ADD and ADHA in children. The drug is well absorbed throughout the gastrointestinal tract. However, it has an extremely short half-life, which necessitates a multi-dose treatment regimen for conventional (immediate release) dosage forms such as currently available 5, 10, and 20 mg tablets. Due to high C_{max} , oral administration of 10 and 20 mg Ritalin® is reported to result in notable side effects such as anorexia, weight loss, dizziness, etc. Furthermore, it requires the hyperactive children to be dosed in school thus causing hardship to school authorities as well as parents. The drawback of Methylphenidate is that it also produces a euphoric effect when administered intravenously or through inhalation, thus presenting a high potential for substance abuse. Sustained release formulations for once-a-day dosing, such as 20 mg Ritalin SR® tablets currently available from Novartis and Geneva (generic version), were developed with the objective of providing efficacy for 8 hours, thereby improving compliance and reducing the incidence of diversion. However, there are reports which strongly suggest that the sustained release formulations exhibit a slower onset of action/efficacy compared to the immediate release dosage forms (W.E. Pelham et al., "Sustained Release And Standard Methylphenidate Effects On Cognitive And Social Behavior In Children With Attention Deficit Disorder," Pediatrics, Vol. 80, pp 491-501 (1987).

[0002] Recently, OROS® (Methylphenidate HCl) has been approved by FDA. It is a new osmotic controlled release once-a-day oral dosage form with a drug overcoat, that is designed to deliver a portion of the dose for rapid onset of action and deliver the remainder of the dose in a controlled manner for about 10 hours. The manufacturing cost of this complicated dosage form is expected to be very high and hence resulting in a high cost of treatment. Hence, there is a dire need to develop modified release dosage forms with moderate cost of goods and having not only a rapid onset of action but also with a significantly longer duration of action.

[0003] U.S. Patent No. 5,908,850 assigned to Celgene Corporation discloses a method for treating children with the above disability to be treated using a sustained release dosage form containing d-threo-methylphenidate or pharmaceutically acceptable salts thereof thus minimizing hyperactivity and side effects. However, it does not address how it avoids dosing in school, thereby minimizing potential drug abuse.

[0004] WO 00/35426 discloses an oral controlled release formulation of methylphenidate hydrochloride based on a gelatine capsule containing multiple methylphenidate beads which have immediate release and controlled release properties.

[0005] It has been amply demonstrated that by administering two-bead capsule dosage forms manufactured in accordance with the present invention, therapeutically efficacious plasma concentrations can be achieved for rapid onset of action and maintained for over a 12-hour period, thus eliminating the need to dose children in the school.

SUMMARY OF THE INVENTION

[0006] The present invention provides a modified release methylphenidate hydrochloride capsule drug delivery system comprising a multitude of IR (immediate release) and ER (extended release) beads filled into capsules at a ratio of 10 IR/90 ER to 50 IR/50 ER beads each of said IR and ER beads containing about 5 to 20% w/w methylphenidate hydrochloride, wherein the IR bead is an inert sugar core particle layered with methylphenidate containing a binder at a concentration of 0.5 to 5 weight %, said layered particle further being coated with a seal coat in an amount up to 4% w/w, and wherein the ER bead comprises an IR bead coated with a dissolution rate controlling polymeric coating in an amount from 5 to 25% by weight based on the total weight of the coated particle, the ER bead being seal coated in an amount up to 4% w/w, wherein the sealcoat is hydroxypropylmethylcellulose (HPMC).

[0007] An object of the present invention is to provide a method for manufacturing pharmaceutically elegant multi-particulate dosage forms based on the Difficaps® technology, having two types of bead populations - one immediate release (IR) Bead and the other extended release (ER) Bead. The IR Bead is designed to release all of the dose over a short period of time, preferably within 30 minutes to act as a bolus dose for rapid onset of action. In contrast, the ER Bead is designed to release the remainder of the total dose as a desired profile over a 12-hour period when dissolution tested in water by USP Apparatus 2 (Paddles @ 50 rpm). Testing to determine *in vitro/in vivo* correlations can be conducted to predict desirable profiles which can be expected to maintain blood levels of the active agent within a desired therapeutic range over an extended period of time. Another objective is

to provide a novel multi-particulate dosage form in order to minimize side effects and eliminate the need to dose children with ADD and ADHD in the school, the release rates from ER Beads and the ratio of IR to ER Beads being determined based on the *in vitro/in vivo* correlations and efficacy study results obtained.

BRIEF DESCRIPTION OF THE DRAWINGS

[0008]

Fig. 1 is a graph showing the mean plasma concentration profile for various dosage forms described in example 2;

Fig. 2 is a graph showing the mean methylphenidate plasma concentrations versus time profiles for the dosage forms described in example 4;

Fig. 3 is a graphical representation of the stability data for modified release methylphenidate hydrochloride capsules, 20 mg (30 IR/70 ER Beads) at 30° C/60% RH; and

Fig. 4 is a graphical representation of the stability data for modified release methylphenidate hydrochloride capsules, 20 mg (30 IR/70 ER Beads) at 40°C/75% RH.

DETAILED DESCRIPTION OF THE INVENTION

[0009] The active core of the novel dosage form of the present invention may be comprised of an inert particle such as a commercially available non-pareil sugar sphere. Methylphenidate is layered on the sugar spheres from an aqueous solution of the drug and a binder such as polyvinylpyrrolidone (PVP). "Methylphenidate" as used herein includes all optical isomers of the compound and all pharmaceutically acceptable salts thereof. The drug layered beads are provided with up to 4%, preferably up to 2% w/w seal coat using the film-former hydroxypropylmethylcellulose (HPMC) (e.g., Opadry Clear) to produce IR Beads.

[0010] ER Beads are produced by coating IR Beads with a solution or an aqueous dispersion of a dissolution rate controlling polymer thereby forming an extended release membrane coating on the IR bead. Examples of dissolution rate controlling polymers include, but are not limited to, ethylcellulose (e.g., Aquacoat® ECD-30), neutral copolymers based on ethylacrylate and methylmethacrylate, and copolymers of acrylic and methacrylic acid esters having quaternary ammonium groups. The membrane coated beads are also typically seal coated with HPMC to produce Extended Release (ER) Beads. The IR and ER Beads are filled into hard gelatin capsules at predetermined ratios to produce modified release (MR) Beads. Ratios found to provide desirable release profiles ranges from about 10IR/90ER to 50IR/50ER, preferably from 20IR/80ER to 40IR/60ER, and most preferably at a ratio of 30IR/70ER.

[0011] The amount of drug layered on the core (sugar sphere) can be varied widely. A typical dose is expected to be from about 10 to 40 mg of active drug. IR beads typically will account for about 20 to 40% of the dose. Due to limitations in accurately dosing small fill weights into capsules in a two-bead capsule filling equipment, the drug content in the drug layered beads may range from 5 to 20% w/w. Those skilled in the art will be able to select an appropriate amount of drug for coating onto the core to achieve the desired dosage. Generally, the dissolution rate controlling polymeric coatings on the active core particle vary from 5 to 25%, preferably from 5 to 20% and more preferably from 5 to 10% by weight based on the total weight of the coated particle, depending on the coating materials and solvents selected.

[0012] The thickness of the membrane layer or the type of polymer selected depends on the desired release profile, and is optimized for achieving a desired *in vitro* release profile, which is predicted based on the *in vitro/in vivo* correlations and efficacy study results. Preferably, the release profile provides an immediate bolus of drug and extended release of the drug at a relatively constant rate for an extended period of time (over 12 hours or more). The unit dosage form according to the present invention may comprise one bead population, which provides only an extended release profile. Alternately, it may consist of an IR bead population that provides a short-duration (sustained release) bolus component of the dose by optionally coating IR Beads with a mixture of water insoluble and water soluble polymers at a ratio of 95/5 to 70/30.

[0013] The invention also provides a method of manufacturing a modified release methylphenidate dosage form having a mixture of two bead populations which comprises the steps of:

1. 1. coating an inert particle such as a non-pareil seed with methylphenidate and a polymeric binder and coating said drug layered core particle with a seal coat to form IR beads, wherein the sealcoat is hydroxypropylmethylcellulose (HPMC), to form IR Beads, which may be present in the unit dosage form to act as a bolus dose;
2. 2. coating said particle with a plasticized solution or suspension of a water insoluble polymer or a mixture of water soluble and water insoluble polymers, coating said beads with a seal coat, wherein the sealcoat is hydroxypropylmethylcellulose (HPMC) and curing at high temperatures (e.g., 50° - 70°C) for 4 to 12 hours, to form extended release (ER) Beads; and
3. 3. filling into hard gelatin capsules beads of (1) and/or (2) at a ratio of 20IR/80SR to 40IR/60SR Beads, each capsule containing 10 to 40 mg methylphenidate hydrochloride.

[0014] An aqueous or a pharmaceutically acceptable solvent medium may be used for preparing drug containing core particles. The type of film forming binder that is used to bind the water soluble drug to the inert sugar sphere is not critical but usually water soluble, alcohol soluble or acetone/water soluble binders are used. Binders such as polyvinylpyrrolidone (PVP), polyethylene oxide, hydroxypropyl methylcellulose (HPMC), hydroxypropyl cellulose (HPC), polysaccharides such as dextran, corn starch may be used at concentrations of 0.5 to 5 weight %. The drug substance may be present in this coating formulation up to 55 weight %, preferably up to about 40% weight %, and most preferably up to about 20% weight, depending on the viscosity of the coating formulation.

[0015] Dissolution rate controlling polymers suitable for incorporating in the formulation for producing ER Beads are selected from the group consisting of ethylcellulose (or e.g., Aquacoat® ECD-30), neutral copolymers based on ethylacrylate and methylmethacrylate, copolymers of acrylic and methacrylic acid esters having quaternary ammonium groups, polyvinyl acetate/crotonic acid copolymer and combinations thereof.

[0016] Dissolution rate controlling polymers used in forming the membranes are usually plasticized. Representative examples of plasticizers that may be used to plasticize the membranes include triacetin, tributyl citrate, trimethyl citrate, acetyl tri-n-butyl citrate diethyl phthalate, castor oil, dibutyl sebacate, acetylated monoglycerides and the like or mixtures thereof. The plasticizer may comprise about 3 to 30 wt. % and more typically about 10 to 25 wt% based on the polymer. The plasticizer is selected based on the total solids in the coating system (dissolved or dispersed) and depends on the polymer or polymers and the nature of the coating medium. Generally, this will be between 5 and 40 weight percent based on the total weight of the coating system.

[0017] The release characteristics of the IR Beads can optionally be further modified to provide a short duration (sustained release) bolus dose. The IR Beads in this embodiment are coated with a mixture of a water insoluble polymer such as ethylcellulose and a water soluble polymer such as low molecular weight HPMC, HPC, methylcellulose, polyethylene glycol (PEG) at a thickness of from 1 weight % up to 5 weight % depending on the solvent or latex dispersion based coating formulation used. The water insoluble polymer to water soluble polymer ratio may typically vary from 95:5 to 70:30.

[0018] The following non-limiting examples illustrate the dosage formulations in accordance with the invention.

Examples

[0019] Modified Release (MR) Capsules of Methylphenidate Hydrochloride, a ADD or ADHD drug, consist of a mixture of two sets of beads: The first set is referred to as immediate release (IR) Beads. IR Beads are designed to provide a loading or bolus dose by releasing all of the methylphenidate hydrochloride within the first hour, preferably within the first 30 minutes. The second set is referred to as the Extended Release (ER) Beads. ER Beads are designed to release methylphenidate slowly over a period of 10-12 hours.

[0020] In a preferred embodiment, IR Beads are prepared by adding Methylphenidate HCl to an aqueous binder solution, preferably a PVP solution. Sugar spheres are coated with the drug solution and then dried. The drug containing particles are coated with a sealcoat of HPMC (Opadry Clear) to form IR Beads in accordance with the invention. Release characteristics of the IR Beads can be modified by optionally coating IR Beads with a blend of a water soluble polymer such as HPMC and a water insoluble polymer such as ethylcellulose.

[0021] The ER Beads are produced by applying a layer of extended release membrane coating (with a dissolution rate controlling polymer such as ethylcellulose) and then a seal coat on IR Beads. The two sets of beads when filled into capsule shells at an appropriate ratio will produce the target *in vitro* release profile which in turn will result in plasma concentrations required to provide rapid onset of action and efficacy over several hours in school going children with ADD or ADHD

Example 1:

[0022] Methylphenidate HCl (200 g) was slowly added to an aqueous solution (about 15 % solids) of polyvinylpyrrolidone (10 g Providone K-30) and mixed well. 25-30 mesh sugar spheres (770 g) were coated with the drug solution in a Versa Glatt fluid bed granulator. The drug containing pellets were dried, and a sealcoat of Opadry Clear (20 g) was first applied to produce IR Beads. ER Beads are produced by taking IR Beads and coating with the dissolution rate controlling polymer. A plasticized ethylcellulose coating was applied to the methylphenidate particles (893 g) by spraying Aquacoat® ECD-30(233 g) and dibutyl sebacate (16.8 g). An outer seal coating formulation (20 g) of Opadry was sprayed onto the coated active particles. The coated particles were cured at 60°C for 12 hours so that polymer particles coalesce to form a smooth membrane on ER Beads.

[0023] The IR and ER Beads were then filled into hard gelatin capsules using an MG Capsule Filling Machine with dual bead filling hoppers. Three clinical batches, Methylphenidate HCl MR Capsules, 25 mg (20 IR/80 ER Beads), 25 mg (30 IR/70 ER Beads) and 25 mg (40 IR/60 ER Beads), were manufactured, tested, and released for pilot biostudies. The dissolution profiles of these capsules are presented in Table 1 showing increasing release rates with increasing IR Bead fraction in the finished capsule.

Table 1: Dissolution Data for Example 1

Time, Hours	(20 IR/80 ER Beads)	(30 IR/70ER Beads)	(40 IR/60 ER Beads)
0.0	0.0	0.0	0.0
1.0	24.5%	31.6%	42.1%
2.0	29.8%	37.4%	48.3%
4.0	57.8%	59.0%	66.3%
8.0	79.2%	76.3%	83.5%
12.0	89.1%	84.6%	88.2%

Example 2:

[0024] In order to evaluate the bioavailability of the pilot clinical supplies manufactured as described in Example 1 and to establish *in vitro*/*in vivo* correlations, a randomized, open-labelled, six-period crossover biostudy was conducted in 24 healthy subjects, of which 18 subjects completed the study. Treatment regimens included a single oral dose of (A) one 10 mg Ritalin® IR tablet, (B) one 10 mg Ritalin IR tablet at 0 and 4 hours, (C) one 20 mg Ritalin® SR tablet, (D) one 25 mg MR Capsule (20 IR/80 ER Beads), (E) one 25 mg MR Capsule (33 IR/70 ER Beads), and (F) one 25 mg MR Capsule (40 IR/60 ER Beads). Pharmacokinetic assessments were made by measuring serial plasma methylphenidate concentrations after administration of each formulation. Each of the treatments administered resulted in a unique mean plasma concentration profile (Figure 1). Treatments A, B, and C appeared to have similar elimination rate processes. In contrast, treatments D, E, and F appeared to have similar but slower elimination rate processes, implying that the methylphenidate elimination following the administration of Treatments D, E, and F is limited by the release rate from the MR capsule. Based on the study results, the Treatment F met the bioequivalence confidence interval requirements with Treatment C, the 20 mg methylphenidate SR formulation, suggesting the need for a faster release rate from the dosage form manufactured in accordance with the present invention.

Example 3:

[0025] Methylphenidate HCl (1,168.4 g) was slowly added to a solution of polyvinylpyrrolidone (58.4 g Providone K-30) in 7,536 g of purified water and mixed well. 25-30 mesh sugar spheres (4,500 g) were coated with the drug solution in a Glatt fluid bed granulator GPCG 5. The drug containing pellets were dried, and a sealcoat of Opadry Clear (121.7 g) in 1,400 g purified water was first applied. The dissolution rate controlling polymer coating was applied to the active particles (4,500 g) by spraying a dispersion of Aquacoat ECD (1,187.4 g) and dibutyl sebacate (85.5 g) in 199.5 purified water. An outer seal coating formulation (Opadry)(101.8 g) in 1,170.7 g purified water was sprayed onto the coated active particles. The coated particles were cured at 60°C for 12 hours so that the polymers were coalesced to produce ER Beads.

[0026] An IR Bead batch (Batchsize: 5,535.6 g) at 10% drug load was also prepared by following the above procedure. Methylphenidate MR Capsules, 20 mg (30 IR/70 ER) Batch (6000 size #3 capsules), containing 6.0 mg of IR Beads and 14 mg of ER Beads were manufactured using MG2 Futura capsule filling equipment. Similarly, Methylphenidate HCl MR Capsules, 20 mg (40 IR/60 ER Beads) Batch, were manufactured.

Table 2: Dissolution Data for Example 3

Time, Hours	(30 IR/70ER Beads)	(40 IR/60 ER Beads)
0.0	0.0	0.0
1.0	33.4%	41.3%
2.0	44.9%	50.9%
4.0	66.2%	69.6%
8.0	87.1%	89.2%
12.0	97.1%	98.0%

Example 4:

[0027] A randomized six-way crossover study in 24 healthy children with ADHD (Protocol MAI 1001-02) was performed using 20 mg MR Capsules (30 IR/70 ER Beads and 40 IR/60 ER Beads of Example 3) and 2 x 20 mg dosed to children in the fed condition in comparison with Ritalin IR 10 mg dosed twice. The plasma profiles were obtained in a randomized, two-double-blind, crossover comparison of IR bid and placebo in stage 1 and two doses of two MR capsules in stage 2 in 24 healthy children. Children received MR capsules (30 IR/70 ER and 40 IR/60 ER Beads of Example 3, single and double doses) and one dosing regimen of Ritalin IR tablets (10 mg bid). Mean methylphenidate Plasma concentrations versus Time profiles are presented in Figure 2. A level A correlation was established between the *in vitro* release and *in vivo* absorption with a correlation coefficient of $r^2 = 0.98$ and a slope of almost 1, as per the FDA guidelines, Guidance for Industry: Extended Release Oral Dosage Forms.

Example 5:

[0028] Methylphenidate HCl (11.7 kg) was slowly added to an aqueous solution of polyvinylpyrrolidone (500 g Providone K-30) and mixed well. 25-30 mesh sugar spheres (38.5 kg) were coated with the drug solution in a fluid bed equipment, Fluid Air FA 0300. The drug containing pellets were dried, and a sealcoat of Opadry Clear (2% w/w) in purified water was first applied. The dissolution rate controlling polymer coating was applied to the active particles (8.6% w/w) by spraying a dispersion of Aquacoat ECD and dibutyl sebacate. An outer seal coat of Opadry Clear (2% w/w) was applied onto the coated active particles. The coated particles were cured at 60°C for 12 hours so that the polymers were coalesced to produce ER Beads. An IR Bead batch (Batchsize: 50.4 kg) at about 10% drug load was also prepared by following the above procedure. Methylphenidate MR Capsules, 20 mg in size #3 capsules, containing 6.0 mg of IR Beads and 14 mg of ER Beads were manufactured using an MG Futura capsule filling equipment. Similarly, Methylphenidate HCl MR Capsules, 10 mg (30 IR/70 ER Beads) and 30 mg (30 IR/70 ER Beads), were also manufactured. The initial and up to 18-month stability data at 30°C/60% RH and up to 6-month stability data at 40°C/75% RH for MR Capsules, 20 mg, are presented, respectively, in Figures 3 and 4. Both 10 and 30 mg capsule products at the ratio of 30 IR/70 ER Beads have also demonstrated to be physically and chemically stable.

Example 6:

[0029] Methylphenidate HCl (2,336.8 g) was slowly added to an aqueous solution of polyvinylpyrrolidone (116.8 g Povidone K-30) in 14,072 g of purified water and mixed well. 25-30 mesh sugar spheres (9,000 g) were coated with the drug solution in a Glatt fluid bed granulator GPCG 5. The drug containing pellets were dried, and a sealcoat of Opadry Clear (243.4 g) in 2,800 g purified water was first applied. The dissolution rate controlling polymer coating was applied to the active particles (9,500 g) by spraying a solution of ethylcellulose and diethyl phthalate in 98/2 acetone/water. The coated ER Beads were cured at 60°C for 4 hours. IR Beads were prepared by following above procedure. The IR and ER Beads were filled into capsules at a ratio of 30 IR/70 ER Beads.

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US5908850A [0003]
- WO0035426A [0004]

Non-patent literature cited in the description

- **W.E. PELHAM et al.** Sustained Release And Standard Methylphenidate Effects On Cognitive And Social Behavior In Children With Attention Deficit Disorder *Pediatrics*, 1987, vol. 80, 491-501 [0001]

PATENTKRAV

1. Methylphenidathydrochloridkapsel-lægemiddelindgivelsessystem med modificeret frigivelse omfattende en flerhed af IR- (øjeblikkelig frigivelse) og ER- (længerevarende frigivelse) kugler fyldt i kapsler i et forhold på 10 IR/90 ER- til 50 IR/50 ER-kugler, hvor hver af IR- og ER-kuglerne indeholder
5 ca. 5 til 20 vægt-% methylphenidathydrochlorid, hvor IR-kuglen er en inert sukkerkernepartikel belagt med methylphenidat indeholdende en binder ved en koncentration på 0,5 til 5 vægt-%, hvor den belagte partikel endvidere coates med en tætningscoating i en mængde op til 4 vægt-%, og hvor ER-kuglen omfatter en IR-kugle coatet med en opløsningshastighedsstyrende polymercoating i en mængde fra 5 til 25 vægt-% baseret på den totale vægt af den coatede partikel, hvor ER-kuglen tætningscoates i en
10 mængde op til 4 vægt-%, hvor tætningscoatingen er hydroxypropylmethylcellulose (HPMC).
2. Lægemiddelindgivelsessystem ifølge krav 1, hvor den opløsningshastighedsstyrende polymercoating på ER-kuglen er i en mængde fra 5 til 10 vægt-%.
- 15 3. Lægemiddelindgivelsessystem ifølge krav 1 eller 2, hvor den opløsningshastighedsstyrende polymer på ER-kuglen er udvalgt fra gruppen bestående af ethylcellulose, neutrale copolymerer baseret på ethylacrylat og methylmethacrylat, og copolymerer af acryl- og methacylsyreestere med kvaternære ammoniumgrupper.
- 20 4. Lægemiddelindgivelsessystem ifølge krav 3, hvor den opløsningshastighedsstyrende polymer er ethylcellulose.
5. Lægemiddelindgivelsessystem ifølge et hvilket som helst af kravene 1 til 4, hvor den opløsningshastighedsstyrende polymer er plastificeret.
25
6. Lægemiddelindgivelsessystem ifølge krav 5, hvor den opløsningshastighedsstyrende polymer omfatter ca. 3 til 30 vægt-% plastificeringsmiddel baseret på polymeren.
7. Lægemiddelindgivelsessystem ifølge et hvilket som helst af de foregående krav, hvor binderen
30 er udvalgt fra gruppen omfattende: polyvinylpyrrolidon (PVP), polyethylenoxid, hydroxypropylmethylcellulose (HPMC), hydroxypropylcellulose (HPC), dextran og majsstivelse.
8. Lægemiddelindgivelsessystem ifølge krav 5 eller 6, hvor ER-kuglerne fremstilles ved membrancoating af methylphenidatholdige IR-kugler med en plastificeret opløsningshastighedsstyrende vandopløselig ethylcelluloseformulering som en opløsning eller en vandig dispersion for en
35 vægtstigning på ikke mere end 10 vægt-%.

9. Lægemiddelindgivelsessystem ifølge et hvilket som helst af kravene 5 til 8, hvor plastificeringsmidlet er udvalgt fra gruppen bestående af dibutylsebacat, trimethylcitrat, diethylphthalat, tributylcitrat, triacetin og blandinger deraf.

5 10. Lægemiddelindgivelsessystem ifølge et hvilket som helst af kravene 1 til 9, hvor kapslen omfatter 10 til 40 mg methylphenidat som et hydrochloridsalt bestående af IR- og ER-kugler i et forhold på 20/80 til 40/60.

11. Lægemiddelindgivelsessystem ifølge krav 10, hvor IR- og ER-kuglerne er i et forhold på 30/70.

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12. Fremgangsmåde til fremstilling af et lægemiddelindgivelsessystem til methylphenidathydrochlorid som defineret i krav 1, der omfatter:

a. fremstilling af en lægemiddelbelagt kernepartikel omfattende en vandopløselig methylphenidatholdig filmdannede sammensætning;

15 b. coating af den lægemiddelbelagte kernepartikel med en tætningscoating for at danne IR-kugler, hvor tætningscoatingen er hydroxypropylmethylcellulose (HPMC);

c. coating af IR-kugler med en vandopløselig opløsningshastighedsstyrende polymer fra en vandig dispersion eller en opløsning i acetone/vand for at danne ER-kugler;

20 d. coating af ER-kugler med en tætningscoating, hvor tætningscoatingen er hydroxypropylmethylcellulose (HPMC); hvor vægten af den opløsningshastighedsstyrende polymercoating er fra 5 til 25 vægt-% baseret på den totale vægt af ER-kuglerne; og

e. fremstilling af MR-kapsler ved fyldning af kapsler i et forhold fra ca. 20 IR/80 ER til 40 IR/60 ER for at tilvejebringe en dosis pr. MR-kapsel på fra ca. 10 mg til 40 mg.

25 13. Fremgangsmåde ifølge krav 12, hvor den opløsningshastighedsstyrende polymer er en plastificeret ethylcelluloseformulering.

14. Fremgangsmåde ifølge et hvilket som helst af kravene 12 til 13, hvor forholdet er ca. 30 IR/70 ER.

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DRAWINGS

Group mean plasma concentrations of methylphenidate Study
Protocol # MA1100-01

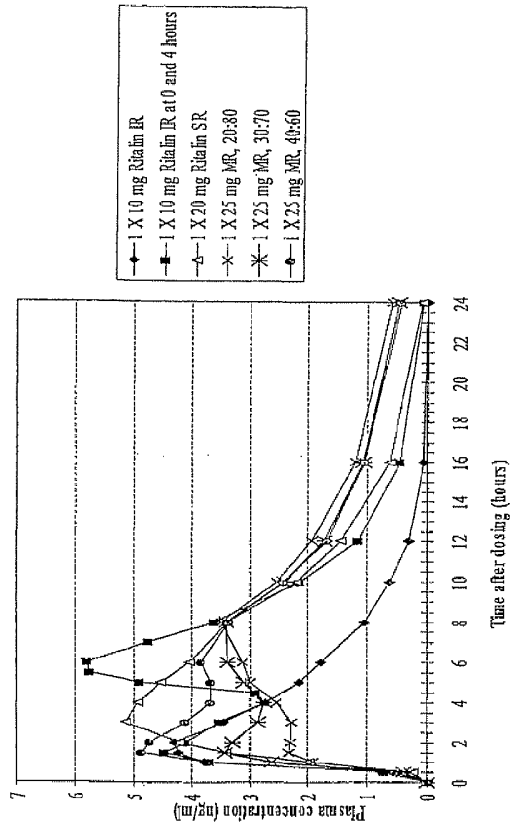


Fig. 1

Group Geometric Mean Plasma Concentrations
Study Protocol # MAI 1001-02

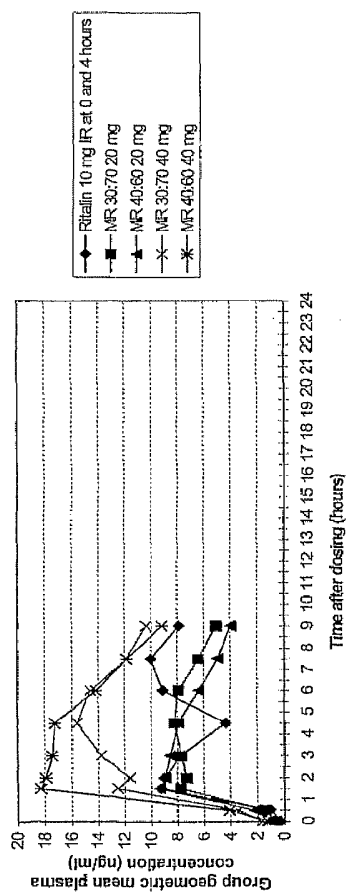


Fig. 2

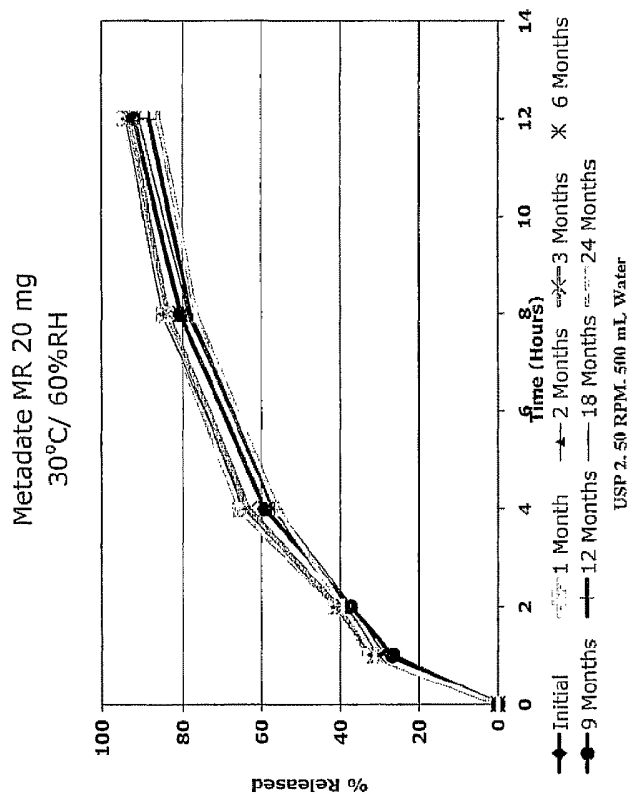


Fig. 3

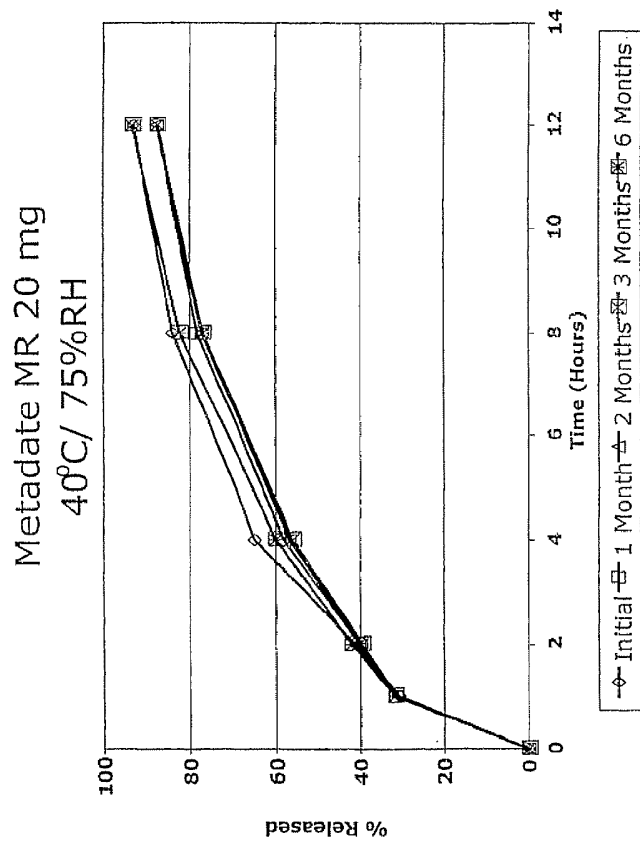


Fig. 4