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(54) **ABLATION BURR**

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(57) **ABSTRACT**

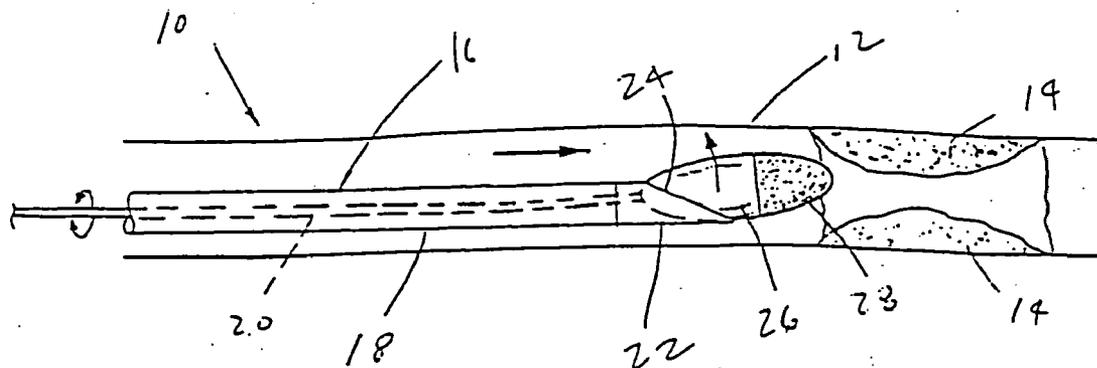
A catheter including an elongate drive shaft having a proxi-  
mal end and a distal end, an ablation burr disposed at the  
distal end expandable between a first position and a second  
position, wherein in the second position has a greater  
transverse dimension than in the first position. The catheter  
of the present invention can include a mechanism for  
positioning the burr eccentrically within a vessel lumen. In  
this context, expansion means that the burr can ablate a  
lumen having a larger diameter than the diameter of the  
lumen of the guide catheter to which the device is advanced.

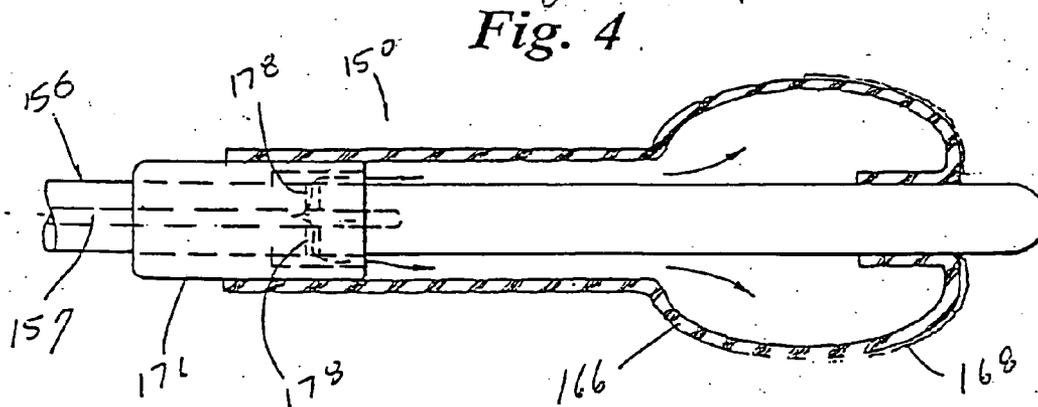
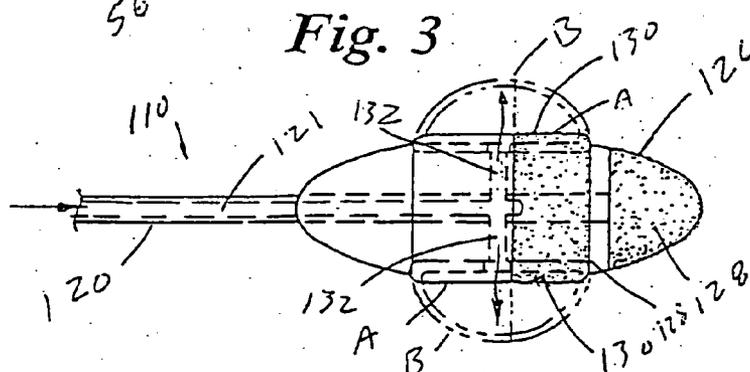
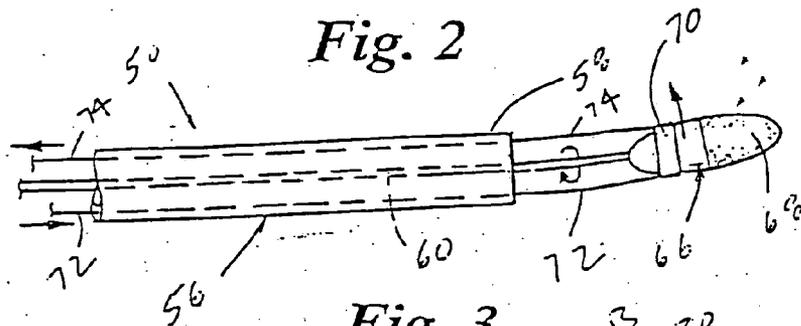
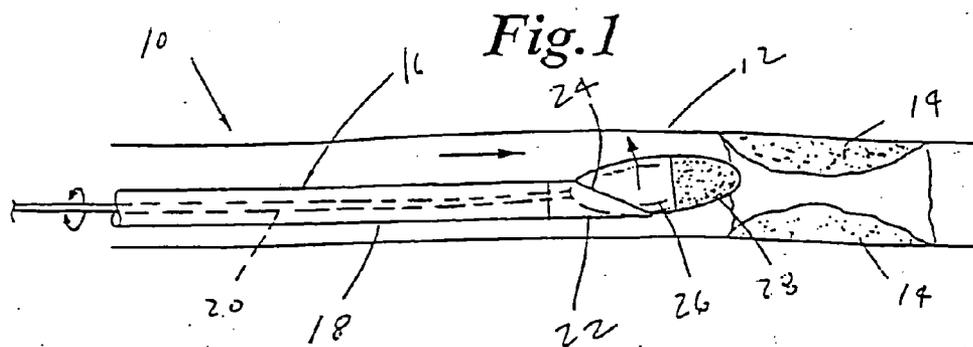
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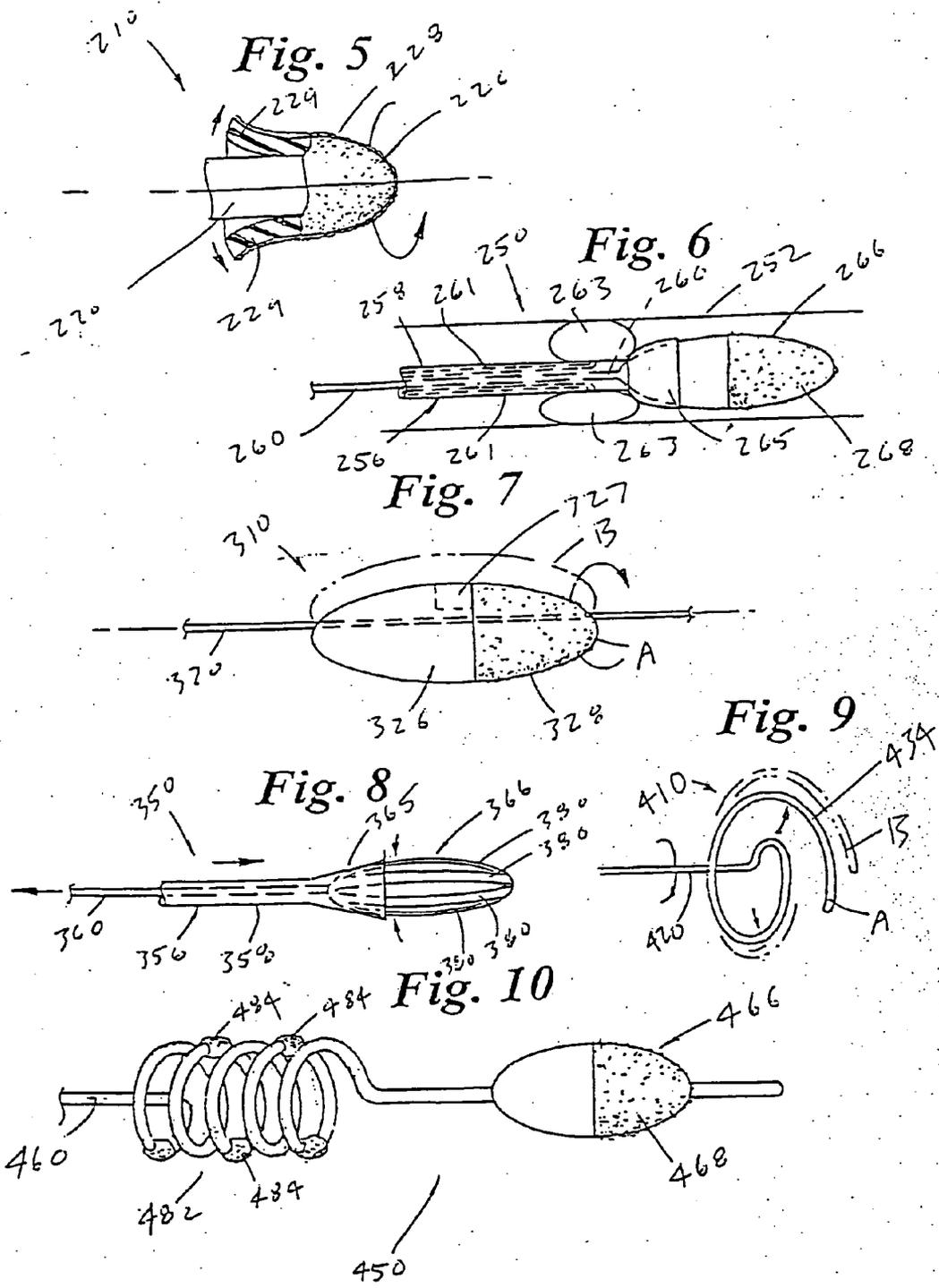
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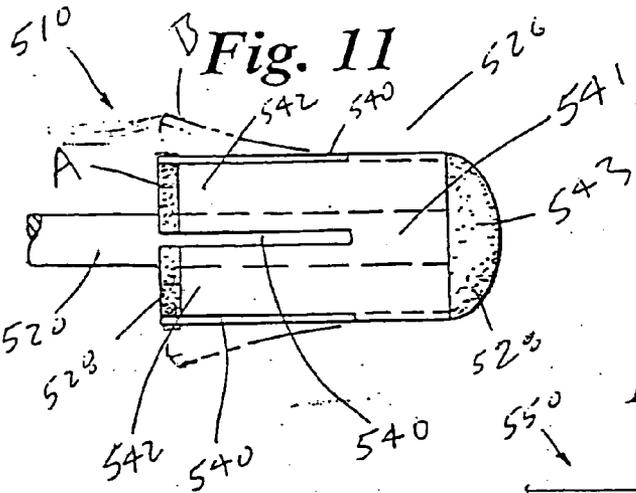


Fig. 12

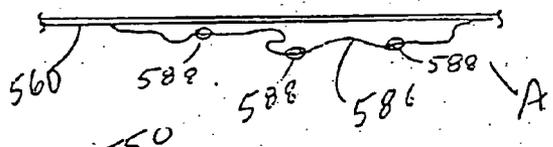


Fig. 13

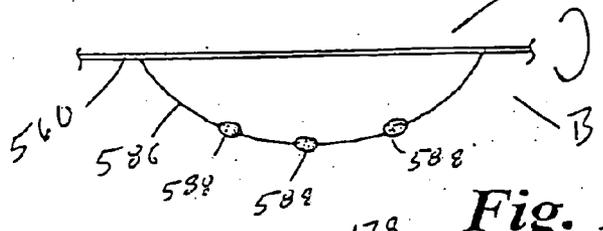
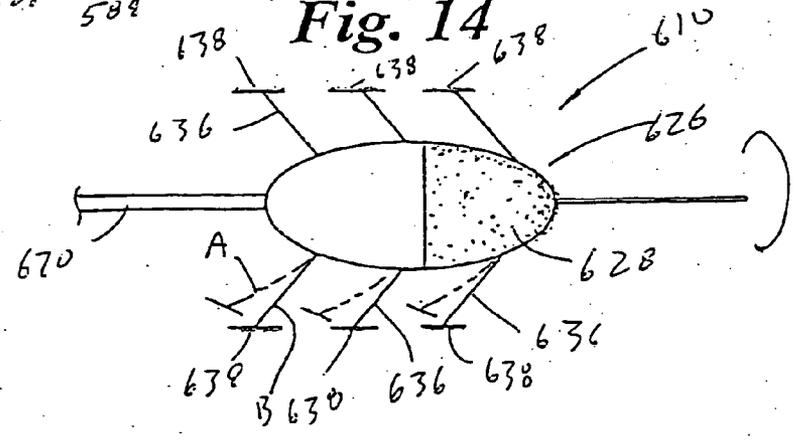
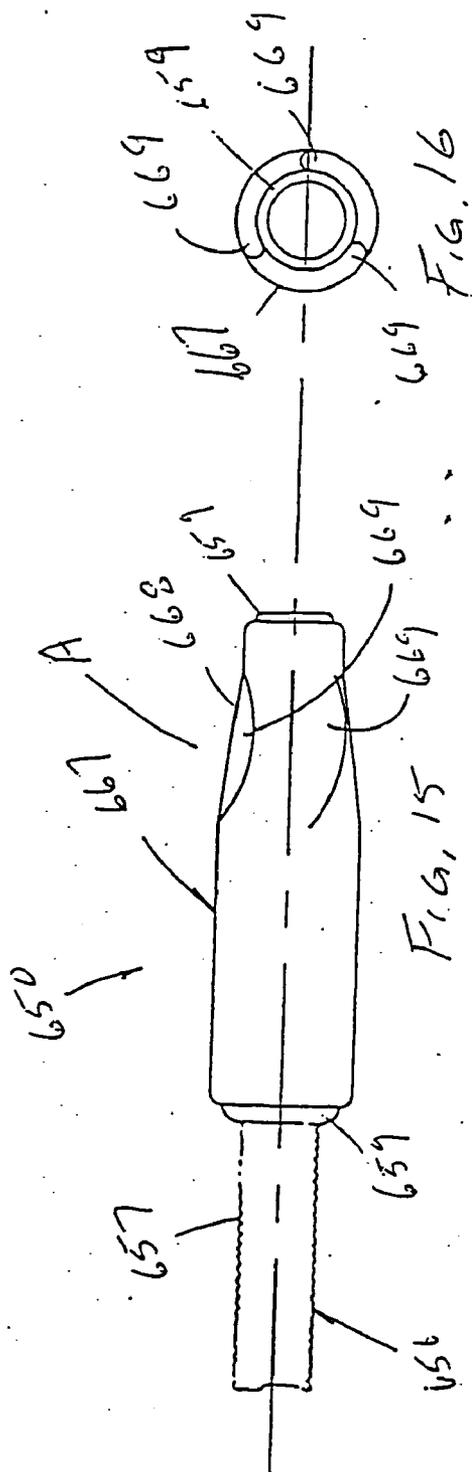
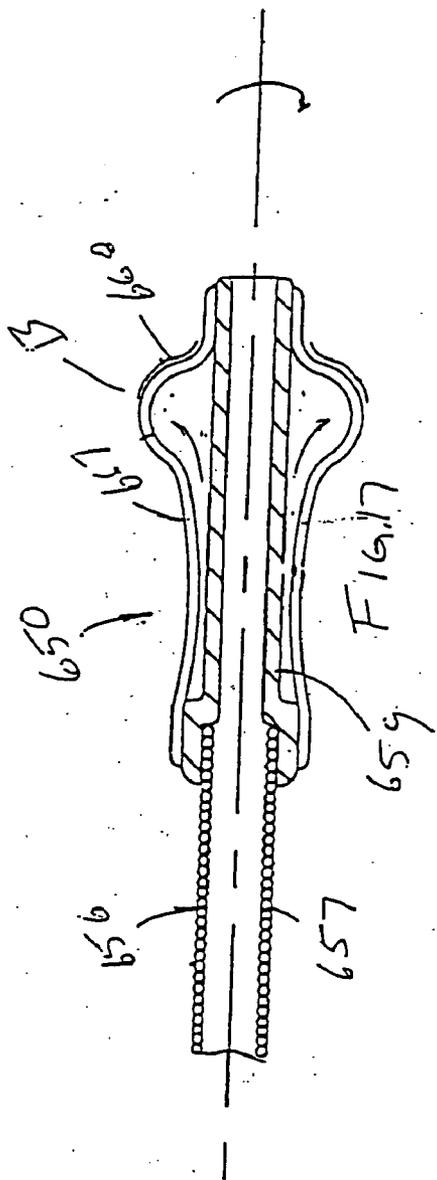
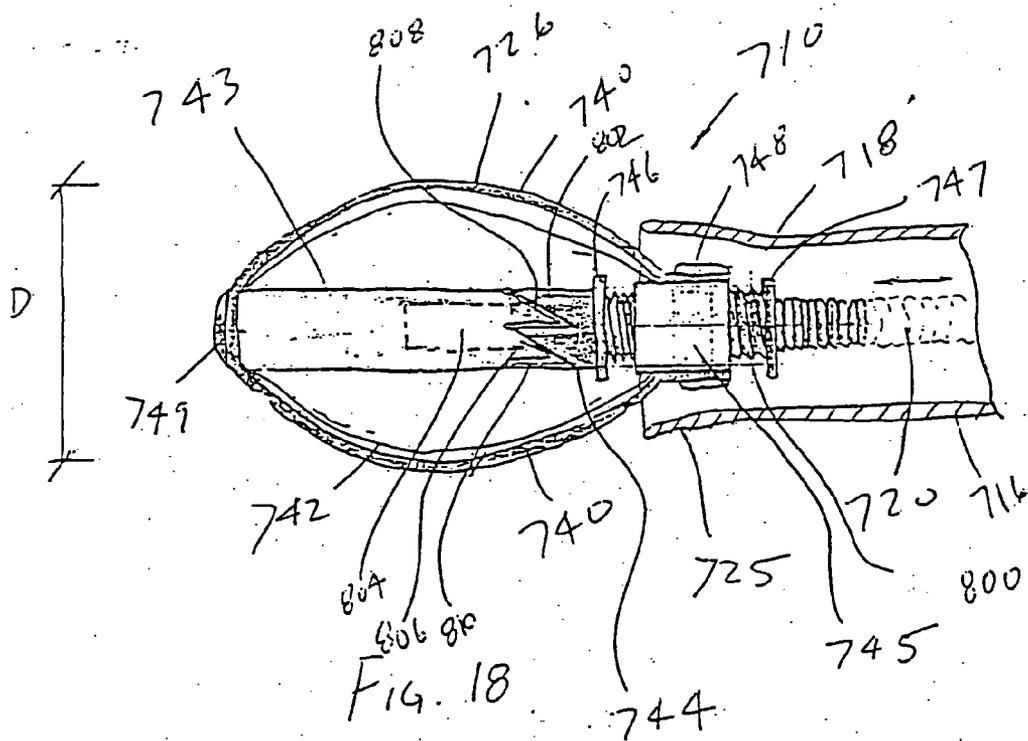


Fig. 14







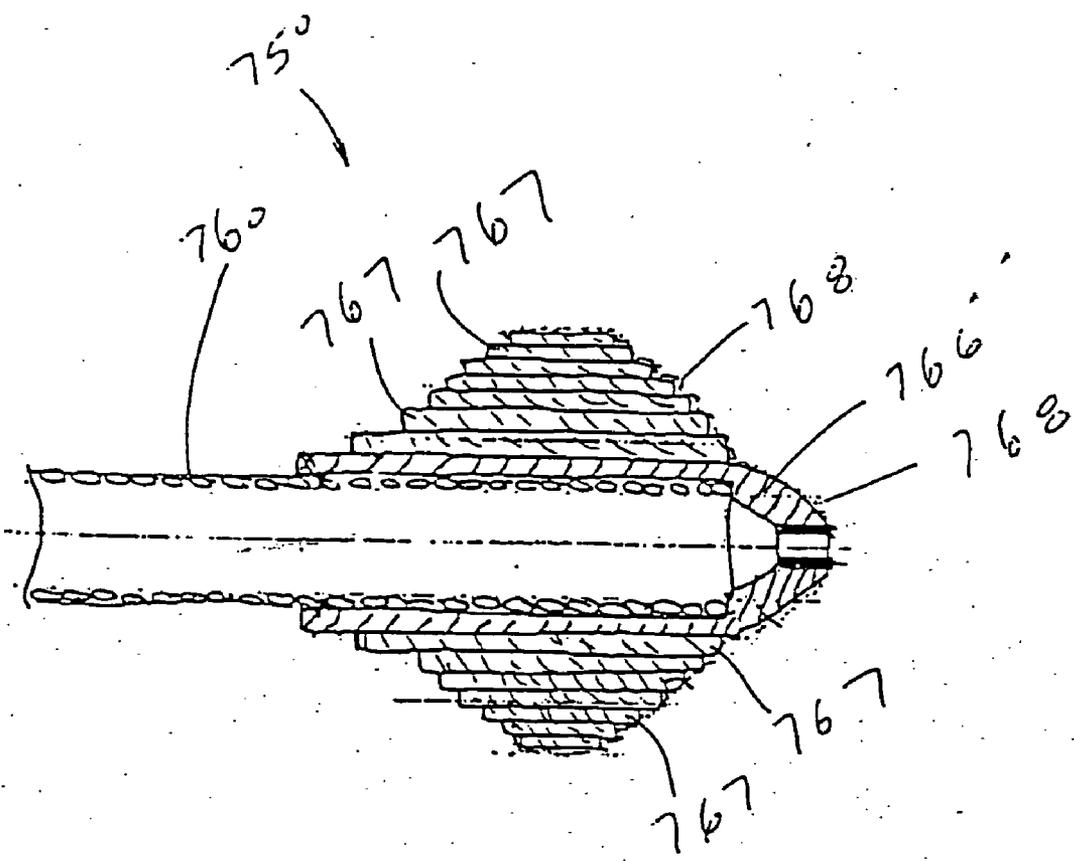


FIG. 19

## ABLATION BURR

### BACKGROUND OF THE INVENTION

[0001] The present invention generally relates to constructions for intravascular treatment devices useful for removing vascular occlusion material from a vascular occlusion or from a vascular lumen. The invention more specifically relates to “expandable” intravascular occlusion material removal devices, as well as to methods of using those devices to treat vascular diseases. In this context, “expandable” means that the burr can ablate a lumen having a larger diameter than the diameter of the lumen of the guide catheter to which the burr is advanced.

[0002] Vascular diseases, such as atherosclerosis and the like, have become quite prevalent in the modern day. These diseases may present themselves in a number of forms. Each form of vascular disease may require a different method of treatment to reduce or cure the harmful effects of the disease. Vascular diseases, for example, may take the form of deposits or growths in a patient’s vasculature which may restrict, in the case of a partial occlusion, or stop, in the case of a total occlusion, blood flow to a certain portion of the patient’s body. This can be particularly serious if, for example, such an occlusion occurs in a portion of the vasculature that supplies vital organs with blood or other necessary fluids.

[0003] To treat these diseases, a number of different therapies are being developed. While a number of invasive therapies are available, it is desirable to develop non-invasive therapies as well. Minimally invasive therapies may be less risky than invasive ones, and may be more welcomed by the patient because of the possibility of decreased chances of infection, reduced post-operative pain, and less post-operative rehabilitation. One type of non-invasive therapy for vascular diseases is pharmaceutical in nature. Clot-busting drugs have been employed to help break up blood clots which may be blocking a particular vascular lumen. Other drug therapies are also available. Further, minimally invasive intravascular treatments exist that are not only pharmaceutical, but also revascularize blood vessels or lumens by mechanical means. Two examples of such intravascular therapies are balloon angioplasty and atherectomy which physically revascularize a portion of a patient’s vasculature.

[0004] Balloon angioplasty comprises a procedure wherein a balloon catheter is inserted intravascularly into a patient through a relatively small puncture, which may be located proximate the groin, and intravascularly navigated by a treating physician to the occluded vascular site. The balloon catheter includes a balloon or dilating member which is placed adjacent the vascular occlusion and then is inflated. Intravascular inflation of the dilating member by sufficient pressures, on the order of 5 to 12 atmospheres or so, causes the balloon to displace the occluding matter to revascularize the occluded lumen and thereby restore substantially normal blood flow through the revascularized portion of the vasculature. It is to be noted, however, that this procedure does not remove the occluding matter from the patient’s vasculature, but displaces it.

[0005] While balloon angioplasty is quite successful in substantially revascularizing many vascular lumens by reforming the occluding material, other occlusions may be difficult to treat with angioplasty. Specifically, some intra-

vascular occlusions may be composed of an irregular, loose or heavily calcified material which may extend relatively far along a vessel or may extend adjacent a side branching vessel, and thus are not prone or susceptible to angioplastic treatment. Even if angioplasty is successful, thereby revascularizing the vessel and substantially restoring normal blood flow therethrough, there is a chance that the occlusion may recur. Recurrence of an occlusion may require repeated or alternative treatments given at the same intravascular site.

[0006] Accordingly, attempts have been made to develop other alternative mechanical methods of minimally invasive, intravascular treatment in an effort to provide another way of revascularizing an occluded vessel and of restoring blood flow through the relevant vasculature. These alternative treatments may have particular utility with certain vascular occlusions, or may provide added benefits to a patient when combined with balloon angioplasty and/or drug therapies.

[0007] One such alternative mechanical treatment method involves removal, not displacement, as is the case with balloon angioplasty, of the material occluding a vascular lumen. Such treatment devices, sometimes referred to as atherectomy devices, use a variety of means, such as lasers, and rotating cutters or ablaters, for example, to remove the occluding material. The rotating cutters may be particularly useful in removing certain vascular occlusions. Since vascular occlusions may have different compositions and morphology or shape, a given removal or cutting element may not be suitable for removal of a certain occlusion.

[0008] Alternatively, if a patient has multiple occlusions in his vasculature, a given removal element may be suitable for removing only one of the occlusions. Suitability of a particular cutting element may be determined by, for example, its size or shape. Thus, a treating physician may have to use a plurality of different treatment devices to provide the patient with complete treatment. This type of procedure can be quite expensive because multiple pieces of equipment may need to be used (such intravascular devices are not reusable because they are inserted directly into the blood stream), and may be tedious to perform because multiple pieces of equipment must be navigated through an often-tortuous vascular path to the treatment site.

### SUMMARY OF THE INVENTION

[0009] The present invention pertains generally to devices for performing atherectomy. In particular, various embodiments of an atherectomy device are disclosed which can ablate a lumen having a larger diameter than the diameter of the lumen of the guide catheter through which the device is advanced.

[0010] In one embodiment, an elongate shaft is provided having a proximal and a distal end. The shaft defines a lumen. A burr deflector is disposed at the distal end of the shaft. The burr deflector includes a burr engaging surface. An elongate rotatable drive shaft extends through the lumen of the first shaft. The drive shaft has a proximal end and a distal end. A burr is disposed at the distal end of the drive shaft. The drive shaft and burr are shiftable relative to the burr deflector. The drive shaft and burr may be shifted between a first position and a second position, wherein the burr is transversely shifted relative to the burr deflector. Preferably, the deflection is co-linear to the length of the drive shaft.

[0011] The burr engaging surface is preferably disposed at an acute angle to the length of the first shaft. The burr preferably includes an engaging surface disposed at an acute angle relative to the drive shaft such that the engaging surfaces provide a path along which the burr can shift transversely relative to the burr deflector.

[0012] In yet another embodiment of a device in accordance with the present invention an elongate shaft is provided which has a proximal and a distal end. The shaft defines a lumen. An elongate rotatable drive shaft extends through the lumen. The drive shaft has a proximal end and a distal end. A burr is disposed at the distal end of the drive shaft. A bushing is disposed around the drive shaft proximate the burr. A steering line is connected to the bushing. The steering line can be pulled by an operator to shift the bushing and thus the burr and drive transversely.

[0013] In yet another embodiment of a device in accordance with the present invention, an elongate rotatable drive shaft is provided having a proximal and a distal end. An ablation burr is disposed at the distal end of the drive shaft. The ablation burr includes a mechanism which expands transversely in response to the centrifugal force generated when the burr rotates.

[0014] In one embodiment, the mechanism is generally tubular and has a proximal end and a distal end constrained against expansion. The central portion of the tubular member is allowed to expand under the influence of the centrifugal force. In yet another embodiment of the mechanism, a member having a generally helical cross-section is provided which tends to unwind, increasing its transverse diameter as the burr rotates. In yet another embodiment of the mechanism, a line is provided having a proximal end and a distal end. The ends of the line are held a distance apart less than the length of the line. An abrasive is disposed on the line. As the burr is rotated, the line moves transversely. In yet another embodiment of the mechanism includes a plurality of bristles which can shift transversely under the influence of centrifugal force.

[0015] In another embodiment of the atherectomy device in accordance with the present invention, an elongate rotatable drive shaft is provided having a proximal end and a distal end. A lumen is defined through the elongate drive shaft. A balloon including an outer surface and defining a balloon enclosure in fluid communication with the inflation lumen is disposed at the distal end of the drive shaft. An abrasive is disposed on the outer surface of the balloon. The balloon can be dilated by pressure or centrifugal force to increase the transverse dimension of the abrasive surface.

[0016] In yet another embodiment of an atherectomy device in accordance with the present invention, an elongate shaft is provided having a proximal end and a distal end. The shaft defines a drive shaft lumen and an inflation lumen. A rotatable drive shaft, having a proximal end and a distal end, is disposed in the drive shaft lumen. An ablating burr is disposed at the distal end of the drive shaft. A balloon is disposed eccentrically on the drive shaft proximate the burr. The balloon can be inflated to push against the vessel wall and shift the drive shaft and burr transversely within the vessel lumen.

[0017] In yet another embodiment of an atherectomy device in accordance with the present invention, an elongate

rotatable drive shaft is provided having a proximal end and a distal end. An ablation burr is eccentrically connected to the drive shaft at the distal end of the shaft. A counterweight is disposed on the burr to place the center of mass of the burr in line with the longitudinal axis of the drive shaft. The presence of the counterweight dampens whipping of the burr which might otherwise occur during rotation of the drive shaft. This embodiment is related to that disclosed in U.S. patent application Ser. No. 08/987,969, filed Dec. 10, 1997 and entitled ASYMMETRIC BURRS FOR ROTATIONAL ABLATION incorporated herein by reference.

[0018] In yet another embodiment of the atherectomy device in accordance with the present invention, an elongate shaft is provided having a proximal end and a distal end. The shaft defines a lumen therethrough. A rotatable drive shaft having a proximal end and a distal end, is disposed through the lumen. A burr, including a plurality of spring members is disposed at the distal end of the drive. The drive shaft and the burr are shiftable between a first position and a second position. In the first position, the spring members are disposed at least in part within the lumen of the first shaft and are transversely constrained thereby. In the second position, the spring members are transversely restrained less than in the first position such that the burr has a greater transverse dimension in the second position than in the first position.

[0019] In yet another embodiment of an atherectomy device in accordance with the present invention, an elongate rotatable drive shaft is provided having a proximal end and a distal end, the drive shaft includes a generally helical-shaped portion proximate the distal end biased to expand when unconstrained. An abrasive is disposed on the helical portion. The helical portion can be advanced to the site where atherectomy will be performed in a constrained and collapsed state through a guide catheter. When the helical shaped portion exits the guide catheter, the helically shaped portion, then unconstrained, will expand transversely.

#### BRIEF DESCRIPTION OF THE DRAWINGS

[0020] FIG. 1 is a side view of a catheter assembly in accordance with the present invention;

[0021] FIG. 2 is a side view of another embodiment of a catheter in accordance with the present invention;

[0022] FIG. 3 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0023] FIG. 4 is a longitudinal, cross-sectional view of yet another embodiment of the catheter in accordance with the present invention;

[0024] FIG. 5 is a fragmentary, cross-sectional view of yet another catheter in accordance with the present invention;

[0025] FIG. 6 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0026] FIG. 7 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0027] FIG. 8 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0028] FIG. 9 is a perspective view of yet another embodiment of the catheter in accordance with the present invention;

[0029] FIG. 10 is a perspective view of yet another embodiment of the catheter in accordance with the present invention;

[0030] FIG. 11 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0031] FIG. 12 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0032] FIG. 13 is a view of the embodiment of FIG. 12 in use;

[0033] FIG. 14 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0034] FIG. 15 is a side view of yet another embodiment of the catheter in accordance with the present invention;

[0035] FIG. 16 is a distal end view of the catheter of FIG. 15;

[0036] FIG. 17 is a cross-sectional view of the catheter of FIG. 15;

[0037] FIG. 18 is a side view of yet another embodiment of the catheter in accordance with the present invention; and

[0038] FIG. 19 is a cross-sectional view of yet another embodiment of the catheter in accordance with the present invention.

#### DETAILED DESCRIPTION OF THE INVENTION

[0039] Referring now to the drawings, wherein like reference numerals refer to like reference elements throughout the several views, FIGS. 1 is a side view of catheter 10 in accordance with the present invention. As shown in FIG. 1, catheter 10 is disposed within vessel 12 proximate a plaque deposit 14. Catheter 10 includes an elongate shaft 16. Shaft 16 includes an outer shaft 18 having a proximal end a distal end and defining a drive shaft lumen therethrough. Catheter 16 also includes a drive shaft 20 having a proximal end a distal end and extending through outer shaft 18. Disposed at the distal end of outer shaft 18 is a burr deflector 22 having a burr engaging surface 24. Disposed at the distal end of drive shaft 20 is a burr 26 rotatable by drive shaft 20, and including an abrasive surface 28.

[0040] As will be appreciated by those skilled in the art, suitable manifold and motor can be provided at the proximal end of catheter 10 to rotate burr 26 and facilitate the uses of catheter 10 as herein described. Those skilled in the art will appreciate the various biocompatible materials available to construct catheter 10 including burr 26. This is also true with respect to the various embodiments of the catheters discussed below. Those skilled in the art will recognize the various manifold, motor, infusion displays control mechanisms and other devices that can advantageously be connected to the proximal ends of the catheter to facilitate their use. Additionally, those skilled in the art will recognize various biocompatible materials, and methods available to construct each embodiment.

[0041] In use, catheter 10 is advanced percutaneously to a coronary lesion including plaque 14. Burr 26 is advanced to plaque as shown by the arrow parallel to shaft 16. Burr 26 is then rotated by drive shaft 26 as shown by the arrows such that plaque deposit 14 is grounded to micro fine particles.

Catheter 10 can be advanced to the lesion through a guide catheter (not shown) having an inner lumen at least slightly greater in diameter than the diameter of burr 26.

[0042] As shown in FIG. 1, the inside diameter of vessel 12 is greater than the diameter of burr 26. In order for burr 26 to be positioned within vessel 12, to remove plaque 14, shaft 10 can be drawn proximally to engage burr 26 against burr deflector surface 24. As burr 26 is forced into surface 24 it will tend to slide proximally along surface 24 while simultaneously being displaced transversely as shown by the arrow on burr 26. The greater the transverse dimension of surface 24, the greater is the possible transverse movement of burr 26. The transverse movement of burr 26 is preferably co-linear with the length of the drive shaft.

[0043] FIG. 2 is a view of an alternate embodiment of an atherectomy catheter 50 in accordance with the present invention. Catheter 50 includes an elongate shaft 56 including an outer shaft 58 defining a drive shaft lumen therethrough. A drive shaft 60 extends through the lumen. Drive shaft 60 includes a proximal end and a distal end. Disposed at the distal end of drive shaft 60 is a burr 66 having an abrasive coating 68. Disposed around a proximal portion of burr 66 is a bushing 70. Bushing 70 can include an inwardly disposed circumferential flange which engages a circumferential groove (not shown) in burr 66 such that bushing 70 is fixedly connected to burr 66, yet burr 66 can rotate within bushing 70. Connected to opposite sides of bushing 70 and extending proximally through shaft 58 are steering wires 72 and 74.

[0044] Catheter 50 can be used as described above with respect to catheter 10. Unlike catheter 10, however, rather than having a burr deflector 22 to transversely move burr 26, burr 60 can be shifted from side to side by pulling proximally a steering wire 72 or 74. Pulling steering wire 74 proximally as steering wire 72 is allowed to move distally will shift burr 66 transversely toward wire 74 as shown by the arrow on burr 66. Similarly, burr 66 can be shifted transversely in the opposite direction by pulling steering wire 72 proximally while allowing wires 74 to shift distally.

[0045] To perform an atherectomy procedure using catheter 50, catheter 50 can be advanced to percutaneously to the site of the lesion through a guide catheter having an inside diameter at least slightly greater than the transverse diameter of burr 66. Burr 66 can be rotated as shown by the arrow proximate drive shaft 60 and be engaged with the lesion. Burr 66 can be moved transversely by steering wires 72 and 74 as necessary to remove the plaque.

[0046] FIG. 3 is a view of yet another embodiment of an atherectomy catheter 110 in accordance with the present invention. Catheter 110 includes an elongate drive shaft 120 having a proximal end and distal end. Drive shaft 120 defines a lumen 121 therethrough. Disposed at the distal end of drive shaft 120 is burr 126 having an abrasive coating 128. Burr 126 includes a generally tubularly shaped member 130 connected to burr 126 at the member's proximal and distal ends. Burr 126 includes lumens 132 in fluid communication with lumen 121 of shaft 120. Lumens 132 lead from lumen 121 to the inside surface of member 130.

[0047] In use, catheter 110 is advanced to a lesion as described above with respect to the other catheter embodiments. Rather than including a mechanism for transversely

shifting a burr however, the tubular member **130** of burr **126** is sufficiently elastic to stretch transversely under the influence of centrifugal force when tip **126** is rotated by shaft **120**. Rotation of tip **126**, thus will move tubular member **130** from a first position A to a second position B. In second position B, burr **126** can ablate a larger diameter path. While member **130** is moving from position A to position B, fluid may be introduced through lumens **121** and **132** as shown by the arrows into the space created inside member **130**.

[0048] FIG. 4 is a cross-sectional view of yet another embodiment of a catheter **150** in accordance with the present invention. Catheter **150** includes an elongate shaft **156** defining an inflation lumen **157**. Disposed proximate the proximal end of shaft **156** is a balloon **166** defining a burr having an abrasive coating **168**. Catheter **150** can include a manifold **176** including lumens **178** in fluid communication with lumen **157** and the interior space of balloon **166**.

[0049] In use, balloon **166** is advanced percutaneously to a lesion. At the lesion, balloon **166** is inflated to increase its diameter. Abrasive surface **168** is then advanced into engagement with the plaque. Balloon **166** is then rotated to abrade plaque.

[0050] FIG. 5 is a partial, cross-sectional view of yet another embodiment of a catheter **210** in accordance with the present invention. Catheter **210** includes an elongate drive shaft **220** having a proximal end and a distal end. A burr **226** is disposed at the distal end of drive shaft **220**. Burr **226** includes an abrasive coating **228** and a distal flexible portion or skirt **229** which is free to move generally transversely under the influence of centrifugal force as burr **226** is rotated by shaft **220**. The arrows proximate skirt **229** show that the direction of the generally transverse movement of skirt **229** to increase the effective diameter of burr **226**. The arrow proximate the distal end of burr **226** shows the rotation of burr **226**. While burr **226** is not rotating skirt **229** can be disposed generally parallel to shaft **220** and then elastically stretch to the position shown in FIG. 5 when burr **226** is rotated.

[0051] FIG. 6 is a side view of yet another alternate embodiment of a catheter **250** in accordance with the present invention. Catheter **250** is shown disposed within a vessel lumen **252**. Catheter **250** includes an elongate shaft **256** having a proximal end and a distal end. Catheter **256** includes an outer shaft **258** which defines the drive shaft lumen and two inflation lumens **261**. An elongate drive shaft **260** is disposed through the drive shaft lumen. A cup shaped bearing **265** is disposed at the distal end of shaft **256**. A burr **266** is connected to the distal end of drive shaft **260**. The distal end of burr **266** can include an abrasive coating **268**. The proximal end of burr **266** can be nested within bearing **265**. Connected to shaft **258** proximate burr **266** are balloons **263**. Balloons **263** define a balloon envelope in fluid communication with inflation lumens **261**. Additional balloons may be used to increase the positional control of burr **266**.

[0052] Catheter **250** is advanced as described above with respect to the alternate embodiments in accordance with the present invention to perform the atherectomy procedure. Likewise, burr **266** is rotated to abrade plaque. In order to shift burr **266** transversely within lumen **252**, balloons **263** may be alternately inflated or deflated to engage the wall of vessel **252** forcing burr **266** transversely in a direction opposite the resultant force of balloons **263** incident the wall of vessel **252**.

[0053] FIG. 7 is a side view of yet another embodiment of a catheter **310** in accordance with the present invention. Catheter **310** includes an elongate shaft **320**. Shaft **320** includes a proximal end and a distal end. A burr **326** is disposed eccentrically on shaft **320** proximate the distal end of shaft **320**. Burr **326** includes an abrasive coating **328**. A counterweight **327** is disposed in burr **326**. The counterweight has a weight sufficient to shift the center of mass of burr **326** such that it lies generally on the longitudinal axis of shaft **320**. The effect of counterweighting can also be achieved by an asymmetrical shaping of the burr and/or creating voids in the burr to shift the distribution of the burrs weight. This allows burr **326** to be rotated by shaft **320** through a position A and B as shown without whipping the distal end of shaft **322**. By eccentrically mounting burr **326** on shaft **320** it can be appreciated by reference to positions A and B that a larger area can be circumscribed by the surface of burr **326** as burr **326** is rotated by shaft **320** than if the burr were rotated about its central axis.

[0054] FIG. 8 is a view of yet another embodiment of a catheter **350** in accordance with the present invention. Catheter **350** includes an elongate shaft **356**. Shaft **356** includes an outer shaft **358** having a proximal end and a distal end and defining a drive shaft lumen therethrough. Shaft **356** also includes a drive shaft **360** disposed through the drive shaft lumen. A cone-shaped bearing **365** is preferably disposed at the distal end of shaft **358**. Bearing **356** has a lumen extending longitudinally therethrough, and having a diameter which generally increases distally. A burr **366** is disposed at the distal end of drive shaft **360**. Burr **366** can have an abrasive coating (not shown). Burr **366** is preferably formed from a plurality of spring members **380** joined at their respective proximal and distal ends. Members **380** are preferably preformed to assume a transversely expanded shape when unconstrained. The diameter of burr **366** can be reduced by withdrawing burr **366** at least in part into bearing **365**. Burr **366** may be withdrawn at least partially into bearing **365** by shifting drive shaft **360** proximally relative to outer shaft **358**. Burr **366** can be advanced to the site of a lesion in the constrained configuration and then expanded, and rotated to abrade plaque.

[0055] FIG. 9 is an embodiment of yet another catheter **410** in accordance with the present invention. Catheter **410** includes a drive shaft **420** having a proximal end and a distal end. A generally spiral shaped ablation burr **434** is disposed at the distal end of drive shaft **420**. Burr **434** can include an abrasive coating (not shown). Upon rotation of drive shaft **420**, burr **434** can generally expand or unwind from a position A to a position B under the influence of centrifugal force. Burr **434** as shown has a generally circular cross section. Burr **434** can have a generally rectangular cross section if burr **434** were formed from a ribbon shaped member.

[0056] FIG. 10 is a view of yet another embodiment of a catheter **450** in accordance with the present invention. Catheter **450** includes an elongate drive shaft **460** having a proximal end and a distal end. A burr **466** is disposed proximate the distal end of shaft **460**. Burr **466** can include an abrasive coating **468**. A coil **482** can be formed in drive shaft **460** proximate burr **466**. Abrasive coating **484** can be deposited on coil **482**. Abrasive coating **484** can be deposited in the configuration and plurality of burrs. Coil **482** can be stretched and flattened to be advanced through a guide

catheter. As the coil portion of drive shaft **460** is advanced distally from a guide catheter, that portion of drive shaft **460** resumes the coil shape shown in **FIG. 10**.

[0057] **FIG. 11** is a view of yet another catheter **510** in accordance with the present invention. Catheter **510** includes drive shaft **520** having a proximal end and a distal end. A burr **526** is disposed at the distal end of drive shaft **520**. Burr **526** preferably includes an abrasive coating **528**. Burr **526** is preferably formed from a generally tubular member **541** which is sealed at its distal end to form an abrasive tip **543**. Longitudinal slits **540** are formed in the proximal end of tubular member **541** such that leaves **542** are disposed therebetween. When burr **526** is rotated, leaves **542** will move from a first position A to a second position B under the influence of centrifugal force.

[0058] **FIG. 12** is a view of yet another embodiment of a catheter **550** in accordance with the present invention. Catheter **550** includes an elongate drive shaft **560** having a proximal end and a distal end. Proximate the distal end of drive shaft **560** is a line **586** having a proximal end and a distal end. The proximal end and distal ends of line **586** are connected to drive shaft **560** at a spaced distance less than the length of line **586**. Abrasive burrs **588** are deposited along line **586**. In **FIG. 12**, line **586** is in a first position A. In **FIG. 13**, line **586** is shown in a second position B wherein line **586** is shift transversely under the influence of centrifugal force as drive shaft **560** is rotated.

[0059] **FIG. 14** is a view of yet another catheter **610** in accordance with the present invention. Catheter **610** includes a drive shaft **620** having a proximal end and a distal end. A burr **626** is disposed proximate the distal end of shaft **620**. Burr **626** preferably includes an abrasive coating **628**. A plurality of bristles extend from burr **626**. Disposed at the outside end of each bristle **636** is a burr end **638** which may include an abrasive coating. Bristles **636** can be configured to move from first position A to second position B under the influence of centrifugal force as burr **626** is rotated. Alternately, bristles **633** may be biased to expand between positions A and B upon becoming unconstrained as they are advanced from a guide catheter.

[0060] **FIG. 15** is a side view of yet another catheter **650** in accordance with the present invention. Catheter **650** includes an elongate drive shaft **656** which can include a proximal, helical shaft encased in a polymer. Shaft **656** can also include a distal shaft portion **659** around which is disposed an elastomeric balloon **667**. Elastomeric balloon **667** includes a distal portion which is folded over into folds or leaflets **669**. The distal end of catheter **650** including the folded region of balloon **667** is preferably coated with an abrasive. **FIG. 16** is a view of the distal end of catheter **650** of **FIG. 15** and offers an alternate view of folds **669**.

[0061] **FIG. 17** is a cross-sectional view of catheter **650** of **FIG. 15**. The arrow to the right of the figure shows the direction of rotation of balloon **667**. In use, as can be seen by comparison of **FIG. 17** with **FIG. 15**, during rotation of balloon **667**, the balloon's distal portion including leaves **669** expands from a first position A to a second position B. This is made possible as the space defined between the balloon inner surface and shaft **659** is preferably preloaded with a fluid such as saline prior to advancement to the site of the lesion. The quantity of fluid preloaded into balloon **667** is such that when balloon **667** is not rotated, it will be

in a relatively reduced diameter, i.e., position A. Whereas, when balloon **667** is rotated, the fluid with shift by centrifugal force into that distal portion of balloon **667** including leaves **669**, expanding balloon **667** into the increased diameter configuration of position B.

[0062] **FIG. 18** shows yet another alternate embodiment of a catheter **710** in accordance with the present invention. Catheter **710** has an elongate shaft **716** having a proximal end and a distal end. Shaft **716** includes an outer sheath **718** defining a drive shaft lumen therethrough. Shaft **716** includes an elongate drive shaft **720** disposed through the lumen. Sheath **718** includes a distal bearing surface which preferably defines a lumen having an inside diameter increasing distally. Disposed at the distal end of drive shaft **720** is an expandable burr **726** which preferably has an abrasive coating (not shown). Burr **726** can be formed from a plurality of spring member similar to the spring members **380** of catheter **350** shown in **FIG. 8**. For clarity, in **FIG. 18**, only two spring members **740** are shown.

[0063] An elastomeric shell is disposed within burr **726** to avoid an increase in hemolysis or platelet aggregation. Shell **742** preferably encloses a main body **743** and unidirectional ratchet **744** including reverse positive stop **746**. A threaded member **800** is threaded into a sleeve **745**. Threaded member **800** is fixably connected at its distal end to stop **746** and fixably connected at its proximal end to forward motion positive stop **747**. Threaded member **800** is also fixably connected to drive shaft **720**. Spring members **740** are connected at their proximal ends to sleeve **745** and fixably held in position by collar **748**. The distal ends of spring members **740** are fixably connected to the distal end of main body **743**. Main body **743** is connected at its proximal end about a pin **804** to ratchet **744**. Ratchet **744** includes teeth **802** and the main body portion includes teeth **806**. Teeth **802** and **806** are shown in **FIG. 8** meshed along angled surfaces **808** and longitudinally extended surfaces **810**.

[0064] In use, ratchet **744** and main body **743** can be used to control the transverse diameter D of burr **726**. For example, a burr advancable through an 8F guide catheter could be expanded between 2.0 mm and 3.5 mm in diameter, at 0.25 mm intervals or steps. The ability to control the diameter of burrs **726** at such steps can be considered indexing. To increase the diameter of burr **726** by indexing, drive shaft **720** can be rotated such that teeth **802** and **806** engage each other along surfaces **808**. Since surfaces **808** are inclined, teeth **806** will tend to rise out from between **802** momentarily increasing the length of burr **726**. As drive shaft **720** continues to rotate, the teeth will index and reengage the adjacent teeth. As ratchet **744** was rotated, stop **746** will have moved toward stay **745** shortening the distance between distal end **749** of burr **726** and sleeve **745**, thus increasing the diameter of burr **726**. This assumes that the spring members **740** bias burr **726** toward its largest diameter. This procedure can be repeated to step wise increase the diameter of burr **726**. It can be appreciated that burr **726** can be kept from rotating during indexing by engagement with sheath **718** or the vessel or vessel lesion. When drive shaft **720** is rotating in the opposite direction to engage teeth **802** and **806** along longitudinally extending surface **810**, burr **726** can be rotated to ablate a lesion.

[0065] The diameter of burr **726** can be reduced by merely withdrawing it at least in part into sheath **718**. Burr **726** can

be withdrawn into sheath 718 sufficiently such that teeth 802 and 806 will be unmeshed. When teeth 802 and 806 are unmeshed, drive shaft 720 can be rotated to advance stop 747 to sleeve 745. At that point, burr 726 is reset to index from its smallest indexing diameter to its largest as described above.

[0066] FIG. 19 is a cross-sectional view of yet another embodiment of a catheter 750 in accordance with the present invention. Catheter 750 includes an elongate drive shaft 760 having a proximal end and a distal end. Drive shaft 760 can be, for example, formed from a helical member surrounded by a polymer sheath. A burr 766 is disposed at the distal end of shaft 760 connected to burr 766 is a loosely spiraled ribbon member 767 which has a reduced length and width as it spirals outwardly from shaft 760. Abrasive coating 768 can also be applied to ribbon member 767. Like the spiraling member 434 of catheter 410 of FIG. 9, ribbon member 767 will tend to unwind and expand transversely when rotated in one direction.

[0067] Numerous advantages of the invention covered by this document have been set forth in the foregoing description. It will be understood, however, that this disclosure is, in many respects, only illustrative. Changes may be made in details, particularly in matters of shape, size, and arrangement of parts without exceeding the scope of the invention. The inventions's scope is, of course, defined in the language in which the appended claims are expressed.

1-22. (canceled)

23. A catheter assembly, comprising:

an elongate drive shaft having a proximal end and a distal end; and

an ablation burr eccentrically connected to the drive shaft at the distal end thereof.

24. The catheter assembly in accordance with claim 23, further comprising a counter weight connected to the burr.

25. The catheter assembly in accordance with claim 23, wherein the burr includes an abrasive surface.

26-31. (canceled)

32. A method of removing lesion material from a patient's blood vessel, comprising the steps of:

routing a catheter through a blood vessel having a central axis, the catheter including an elongate shaft having proximal and distal ends and defining a drive shaft lumen, a driveshaft having proximal and distal ends disposed in the drive shaft lumen, an ablation burr disposed on the distal end of the driveshaft for rotation therewith, and first and second inflation balloons disposed eccentrically on the shaft proximate the burr, wherein inflation of the first balloon urges the ablation burr in a first direction transverse of the central axis of the blood vessel and inflation of the second balloon urges the ablation burr in a second direction transverse of the central axis of the blood vessel;

inflating the first or second balloon to urge the ablation burr in a direction transverse of the central axis of the blood vessel and into contact with lesion material deposited on a sidewall of the blood vessel; and

rotating the burr.

33. The method of claim 32, further comprising:

deflating the first or second balloon; and

inflating the other of the first or second balloon to urge the ablation burr in another direction transverse of the central axis of the blood vessel.

34. The method of claim 32, further comprising supporting a proximal end of the ablation burr.

35. The method of claim 32, wherein the first and second balloons are disposed on opposite sides of the shaft.

36. The method of claim 32, wherein the catheter further includes a bearing positioned at the distal end of the shaft, the bearing defining a bearing surface that is capable of supporting a proximal end of the ablation burr.

37. The method of claim 36, wherein the bearing is cup shaped.

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