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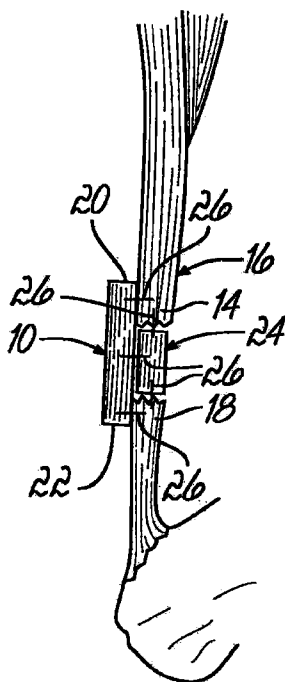


FIG. 5

(57) Abstract: A composition and method for repairing a ruptured connective tissue are disclosed. The composition includes a first biocompatible material to provide a scaffold for connective tissue cell growth and tissue repair. This first biocompatible material may withstand a tensile load of up to 250 N. The composition may also include a second biocompatible material including at least one bioactive agent that can stimulate connective tissue cell growth and tissue repair. The method includes positioning a first end of the first biocompatible material adjacent a first end of a ruptured connective tissue, and positioning a second end of the first biocompatible material adjacent a second end of the ruptured connective tissue. The method may also include positioning the second biocompatible material between the first and second ends of the ruptured connective tissue.

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COMPOSITIONS AND METHODS FOR REPAIR OF CONNECTIVE TISSUE**TECHNICAL FIELD**

[0001] Medical compositions and methods, more particularly, medical compositions and methods for repair of ruptured tendons, ligaments, meniscus, and other connective tissues.

BACKGROUND

[0002] This section is intended to introduce the reader to various aspects of art that may be related to various aspects of the present invention, which are described and/or claimed below. This discussion is believed to be helpful in providing the reader with background information to facilitate a better understanding of various aspects of the present invention. Accordingly, it should be understood that these statements are to be read in this light, and not as admissions of prior art.

[0003] A tendon is a band of fibrous connective tissue that connects muscle to bone and is built to withstand tension. The tendon joins to a muscle at the origin of the tendon. There, collagen fibers from the muscle are continuous with those of the tendon. The tendon inserts into a bone at an enthesis where the collagen fibers are mineralized and integrated into the bone tissue. Tendons transfer the contractions of muscles and can exert an elastic force if stretched.

[0004] The Achilles tendon (also known as the calcaneal tendon) is a tendon of the posterior leg. It serves to attach the calf muscles (lateral and medial gastrocnemius muscle and soleus muscle) and the plantaris muscle to the heel bone (calcaneus).

[0005] Injury to a tendon can occur when the tensile load applied to the tendon exceeds its loadbearing capacity, causing the tendon to rupture. For example, rupture of the Achilles tendon is an injury that commonly occurs in males during sporting activities, generally as an acceleration injury (e.g., pushing off or jumping up). The diagnosis of an acute Achilles tendon rupture is usually straightforward. There is typically a snapping sensation and/or an audible snap in the posterior aspect of the ankle. The subject feels pain and is unable to bear weight due to both pain and weakness.

[0006] Treatment options for a ruptured tendon (such as a ruptured Achilles tendon) include conservative management, percutaneous repair, and open surgical repair. It is believed that open surgical repair provides the best chance for restoration of strength, power, and function of the muscle-tendon-bone complex with the lowest risk for repeat rupture. However, the management of a neglected Achilles tendon rupture poses certain problems to the surgeon as, by the time the

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subject is seen, the tendon ends have often retracted, forming a gap therebetween. Additionally, during surgery, the damaged tendon ends are debrided. Debridement may form a gap, and/or debridement may expand an already-existing gap. In order to treat the tendon to a full recovery, this gap must be closed. Various techniques have been used to eliminate this gap.

[0007] First, a surgeon can pull the two free tendon ends together and affix them to one another with sutures. However, when pulling the two free tendon ends together, each of the tendon ends is stretched. This weakens the tendon by decreasing the amount of tensile load the now-repaired tendon can withstand. This will cause functional deficiency of the tendon later, thereby increasing the likelihood of a repeat rupture.

[0008] Alternatively, portions of the Achilles tendon itself may be used to repair the tendon. For example, a strip of the superficial part of the tendinous portion of the proximal stump of the Achilles tendon may be used to augment repair. This is accomplished by making a posterior longitudinal incision and dissecting a half-inch by seven to nine-inch strip of tendon on a distal pedicle. The strip is then threaded through the trimmed ends of the ruptured tendon and sutured to them. However, this method also may not fully repair the tendon, as part of the tendon itself needs to be stripped away to repair the tendon.

[0009] Alternatively still, additional autologous tissue may be used to "bridge" the two tendon ends. For example, the tendon of the flexor hallucis longus (FHL) muscle of the leg has been used to bridge gaps in ruptured Achilles tendons. The FHL tendon is weaved through the ruptured Achilles tendon ends, and the distal end of the FHL tendon is adhered to the tendon of the flexor digitorum longus muscle of the second toe. Because the FHL tendon is a long tendon, it allows bridging of large Achilles tendon gaps. However, there are drawbacks to this treatment. For example, the process requires not only surgery to repair the ruptured Achilles tendon, but also to obtain the FHL tendon. Further, use of the FHL tendon impairs the normal function of the FHL tendon and FHL muscle. For example, in athletes, the loss of push-off from the toes (particularly the hallux) may cause difficulty when sprinting.

[0010] The tendon of the peroneus brevis muscle has also been used to bridge the gap of a ruptured Achilles tendon. The peroneus brevis tendon is harvested and passed through a transosseous drill hole formed in the heel bone. The peroneus brevis tendon is then passed back onto itself and sutured over the Achilles tendon. Like the use of the FHL tendon, above, use of

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the peroneus brevis tendon has drawbacks. For example, the normal function of the peroneus brevis tendon and peroneus brevis muscle is impaired.

[0011] Additionally, researchers have used human acellular dermal matrix grafts and porcine small intestinal submucosa for bridging tendon gaps in animals. However, these materials only provide a scaffold, but do not promote tendon cell growth and tissue repair to the degree of autologous tissue. Further, small intestinal submucosa can only withstand a small tensile load (approximately 40-50 N). This is much less than the tensile load capability of native tendon. This results in a weakened repaired tendon and the increased likelihood of repeat rupture.

[0012] In view of the drawbacks associated with current compositions and methods for tendon repair, a new and/or improved composition and method for repairing a ruptured tendon is desirable.

SUMMARY

[0013] Certain exemplary aspects of the invention are set forth below. It should be understood that these aspects are presented merely to provide the reader with a brief summary of certain forms the invention might take and that these aspects are not intended to limit the scope of the invention. Indeed, the invention may encompass a variety of aspects that may not be explicitly set forth below.

[0014] One aspect of the present invention provides a composition for bridging a gap in a ruptured tendon. In one embodiment, the composition includes a first biocompatible material that can withstand a tensile load up to 250 N. The first biocompatible material is used to bridge a gap between a first end and a second end of a ruptured tendon. Thus, a first end of the first biocompatible material is associated with the first end of the ruptured tendon, such as by being sutured thereto, and a second end of the first biocompatible material is associated with the second end of the ruptured tendon, such as by being sutured thereto. The first biocompatible material thereby provides a scaffold in proximity to the gap for tendon cell growth and tissue repair.

[0015] In another embodiment, the composition includes a first biocompatible material that provides a scaffold for tendon cell growth and tissue repair, and a second biocompatible material including at least one bioactive agent that can stimulate tendon cell growth and tissue repair. The first biocompatible material is used to bridge a gap between first and second ends of a ruptured

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tendon. Thus, a first end of the first biocompatible material is associated with the first end of the ruptured tendon, and a second end of the first biocompatible material is associated with the second end of the ruptured tendon. The second biocompatible material may be positioned between the first and second ends of the ruptured tendon, and adjacent the first biocompatible material. As stated above, the second biocompatible material includes at least one bioactive agent (e.g., growth factors), which promotes cell growth and tissue repair. This enhances the repair abilities of the composition as compared to providing a scaffold alone.

[0016] Another aspect of the present invention includes a method of repairing a ruptured tendon. In one embodiment, the method includes positioning a first end of a first biocompatible material adjacent a first end of a ruptured tendon and positioning a second end of the first biocompatible material adjacent a second end of the ruptured tendon. The first biocompatible material may then be anchored to the first and second tendon ends, such as by sutures. The method may further generally comprise positioning a second biocompatible material between the first and second ends of the ruptured tendon. The second biocompatible material may also be anchored to the first and second tendon ends and/or to the first biocompatible material. In this manner, the first biocompatible material is used to bridge the gap between the two tendon ends, while the second biocompatible material promotes tissue growth and healing within and/or adjacent the gap.

[0017] Various features discussed below in relation to one or more of the exemplary embodiments may be incorporated into any of the above-described aspects of the present invention alone or in any combination. Again, the brief summary presented above is intended only to familiarize the reader with certain aspects and contexts of the present invention without limitation to the claimed subject matter.

BRIEF DESCRIPTION OF THE DRAWINGS

[0018] The accompanying drawings, which are incorporated in and constitute a part of this specification, illustrate exemplary embodiments of the invention and, together with the summary given above, and the detailed description given below, serve to explain the invention.

[0019] FIG. 1 is a perspective view of a ruptured Achilles tendon.

[0020] FIG. 2 is a perspective view of a first biocompatible material positioned adjacent a ruptured tendon.

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[0021] FIG. 3 is a perspective view of a first biocompatible material positioned adjacent a ruptured tendon and a second biocompatible material positioned adjacent and affixed to the first biocompatible material.

[0022] FIG. 4 is a perspective view of a first biocompatible material positioned adjacent a ruptured tendon and a second biocompatible material positioned adjacent and affixed to first and second ends of the ruptured tendon.

[0023] FIG. 5 is a perspective view of a first biocompatible material positioned adjacent a ruptured tendon and a second biocompatible material positioned adjacent and affixed to the first biocompatible material, and affixed to first and second ends of the ruptured tendon.

DETAILED DESCRIPTION

[0024] One or more specific embodiments of the present invention will be described below. In an effort to provide a concise description of these embodiments, not all features of an actual implementation may be described in the specification. It should be appreciated that in the development of any such actual implementation, as in any engineering or design project, numerous implementation specific decisions must be made to achieve the developers' specific goals, such as compliance with system-related and business-related constraints, which may vary from one implementation to another. Moreover, it should be appreciated that such a development effort might be complex and time consuming, but would nevertheless be a routine undertaking of design, fabrication, and manufacture for those of ordinary skill having the benefit of this disclosure.

[0025] One aspect of the present invention provides a composition for bridging a gap in a ruptured tendon. Referring to the Figures, in one embodiment, the present invention provides a composition that includes a first biocompatible material 10 that can withstand a tensile load up to 250 N. The first biocompatible material 10 is used to bridge a gap 12 between a first end 14 and a second end 18 of a ruptured tendon 16. Thus, a first end 20 of the first biocompatible material 10 is associated with the first end 14 of the ruptured tendon 16, and a second end 22 of the first biocompatible material 10 is associated with the second end 18 of the ruptured tendon 16. The first biocompatible material 10 thereby provides a scaffold in proximity to the gap 12 for tendon cell growth and tissue repair.

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[0026] The first biocompatible material 10 may be substantially nonimmunogenic. Thus, it can be implanted into a subject with minimal chance of provoking an immune response. To achieve this, the first biocompatible material 10 may be acellular. Thus, in one embodiment, the first biocompatible material 10 includes a material or materials that are substantially nonimmunogenic, such as a material chosen from collagen and elastin. In a further embodiment, the first biocompatible material 10 may include both collagen and elastin. However, it will be recognized by those skilled in the art that collagen and/or elastin are merely examples of such materials, and any other substantially nonimmunogenic materials suitable for the composition may be used. For example, such other substantially nonimmunogenic materials may include reconstituted collagen from human or animal sources, and/or may be synthetic, such as Sport Mesh, commercially available from Biomet, Inc. of Warsaw, Indiana.

[0027] Further, the first biocompatible material 10 may be subjected to a process or processes to make it resistant to degradation, such as by enzymes (e.g., collagenase). To that end, in one embodiment, the first biocompatible material 10 may be cross-linked. Such processes are known to those skilled in the art, and exemplary processes may include, but are not limited to, chemical cross-linking and photofixation. Exemplary processes are described in U.S. Patent Nos. 5,397,353; 5,147,514; 5,332,475; 5,817,153, and/or 5,854,397, the disclosures of which is incorporated by reference herein in its entirety. However, other processes known to those of ordinary skill in the art may be used.

[0028] The first biocompatible material 10 may be autogenic, allogenic, or xenogenic with respect to the recipient of the composition. In one embodiment, the first biocompatible material 10 may be xenogenic and includes porcine dermal tissue. In this embodiment, the first biocompatible material 10 particularly may be an acellular scaffold of collagen and elastin, derived from porcine dermal tissue that can be used as a biological implant. The material is cross-linked through a process that makes it resistant to collagenase degradation. This process was described above with respect to U.S. Patent Nos. 5,397,353; 5,147,514; 5,332,475; 5,817,153, and/or 5,854,397. Thus, the first biocompatible material 10 is resistant to degradation and enzymatic attack, and also experiences no sensitization, rejection, allogenicity, or inflammatory response once implanted into a subject. This first biocompatible material 10 is strong and durable, and is readily and consistently colonized by host tissue cells and blood

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vessels. This first biocompatible material 10 may be provided in sheet form, and can withstand a significantly larger tensile load than small intestinal submucosa (SIS) patches (which, as described above, can generally withstand a tensile load of 40-50 N). In various embodiments, the first biocompatible material 10 can withstand a minimum load of 150N, can preferably withstand a tensile load between 150N and 250N, and more preferably can withstand a tensile load of 200N to 250N. In one particular embodiment, the first biocompatible material 10 can withstand a tensile load of up to 250 N. The first biocompatible material 10 may also have a thickness between 0.5 mm and 2.0 mm. In one particular embodiment, the first biocompatible material 10 has a 1.5 mm thickness and preservation of the original collagen structure of the porcine dermal tissue. One suitable first biocompatible material 10 is the Zimmer[®] Collagen Repair Patch, commercially available from Zimmer, Inc.

[0029] In another embodiment, the composition generally includes a first biocompatible material 10 to provide a scaffold for tendon cell growth and tissue repair, and a second biocompatible material 24 including at least one bioactive agent that can stimulate tendon cell growth and tissue repair. Such a bioactive agent may include a growth factor or mixture of growth factors, cytokines, and/or small peptides. The first biocompatible material 10 is used to bridge a gap 12 between first and second ends 14, 18 of a ruptured tendon 16. Thus, a first end 20 of the first biocompatible material 10 is associated with the first end 14 of the ruptured tendon 16, and a second end 22 of the first biocompatible material 10 is associated with the second end 18 of the ruptured tendon 16. The second biocompatible material 24 may be positioned between the first and second ends 14, 18 of the ruptured tendon 16, and adjacent the first biocompatible material 10. As stated above, the second biocompatible material includes at least one bioactive agent (e.g., growth factors, cytokines, small peptides), which promotes cell growth and tissue repair. This enhances the repair abilities of the present composition over those of the prior art.

[0030] As above, the first biocompatible material 10 may be substantially nonimmunogenic to minimize the chance of provoking an immune response. Toward this end, the first biocompatible material 10 may be acellular. Thus, in one embodiment, the first biocompatible material 10 includes a material or materials that are substantially nonimmunogenic, such as a material chosen from collagen and elastin. In a further embodiment, the first biocompatible material 10 may include both collagen and elastin. However, it will be recognized by those skilled in the art that

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collagen and/or elastin are merely examples of such materials, and any other substantially nonimmunogenic materials suitable for the composition may be used. For example, such other substantially nonimmunogenic materials may include reconstituted collagen from human or animal sources, and/or may be synthetic, such as Sport Mesh, commercially available from Biomet, Inc. of Warsaw, Indiana.

[0031] In an alternate embodiment, the first biocompatible material 10 may be subjected to a process or processes to make it resistant to degradation, such as by enzymes (e.g., collagenase). To that end, in one embodiment, the first biocompatible material 10 may be cross-linked. Such processes are known to those skilled in the art, and one such process is described in U.S. Patent Nos. 5,397,353, 5,147,514; 5,332,475; 5,817,153, and/or 5,854,397, the disclosures of which are incorporated by reference herein in their entireties.

[0032] Further still, the first biocompatible material 10 may be autogenic, allogenic, or xenogenic with respect to the recipient of the composition. In one embodiment, the first biocompatible material 10 may be xenogenic and includes porcine dermal tissue. In this embodiment, the first biocompatible material 10 particularly may be an acellular scaffold of collagen and elastin, derived from porcine dermal tissue that can be used as a biological implant. The material may be cross-linked through a process that makes it resistant to collagenase degradation. An exemplary process is described above with respect to U.S. Patent No. 5,397,353, 5,147,514; 5,332,475; 5,817,153, and/or 5,854,397. Thus, the first biocompatible material 10 is resistant to degradation and enzymatic attack. It also may provoke limited or substantially no sensitization, rejection, allogenicity, or inflammatory response once implanted into a subject. The first biocompatible material 10 is strong and durable, and is readily and consistently colonized by host tissue cells and blood vessels. This first biocompatible material 10 may be provided in sheet form, and can withstand a significantly larger tensile load than small intestinal submucosa (SIS) patches (which, as described above, can withstand a tensile load of 40-50 N). In various embodiments, the first biocompatible material 10 can withstand a minimum load of 150N, can preferably withstand a tensile load between 150N and 250N, and more preferably can withstand a tensile load of 200N to 250N. In one particular embodiment, the first biocompatible material 10 can withstand a tensile load of up to 250 N. This is afforded by the first biocompatible material 10 having a thickness between 0.5 mm and 2.0 mm. In one particular

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embodiment, the first biocompatible material includes a 1.5 mm thickness and preservation of the original collagen structure of the porcine dermal tissue. One such first biocompatible material 10 is the Zimmer® Collagen Repair Patch, commercially available from Zimmer, Inc.

[0033] In the embodiment including both first and second biocompatible materials 10, 24, the second biocompatible material 24 includes at least one bioactive agent that can stimulate tendon cell growth and tissue repair. Thus, in various embodiments, the second biocompatible material 24 may include, but is not limited to, at least one of platelet rich plasma (PRP), a collagen-based material, or a hydrogel. Each of these exemplary biocompatible materials may inherently include at least one bioactive agent (e.g., growth factors inherently present in PRP), or at least one bioactive agent may be incorporated into the material (e.g., growth factors added to a hydrogel, such that the hydrogel acts as a vehicle for the growth factors). In one particular embodiment, the second biocompatible material 24 is PRP, and may be autogenously harvested PRP. As is well known to those of ordinary skill in the art, PRP is a source of growth factors that support cell growth and soft tissue healing. It is derived by concentrating platelets and can be added to surgical wounds or grafts to support or speed up the healing process. PRP has previously been used in rotator cuff repair, bone healing, and to enhance ligament and meniscal repair in animals. (See Gamradt, Seth C. M.D.; Rodeo, Scott A. M.D.; and Warren, Russell F. M.D., in *Platelet Rich Plasma in Rotator Cuff Repair*, Techniques in Orthopaedics. Biologics in Shoulder Surgery. 22(1):26-33, March 2007; and Tomasz Mariusz Bielecki and Tadeusz Szymon Gazdzik, in *Percutaneous Injection Of Autogenous Growth Factors In Patient With Nonunion Of The Humerus. A Case Report*, J. Orthopaedics 2006;3(3)e15.)

[0034] PRP includes multiple growth factors. Growth factors, as known to those of ordinary skill in the art, are naturally occurring proteins capable of stimulating cell proliferation and differentiation. PRP generally may include one or more of transforming growth factor (TGF), fibroblast growth factor (FGF), platelet-derived growth factor (PDGF), epidermal growth factor (EGF), and vascular endothelial growth factor (VEGF). TGFs present in PRP particularly include those of the TGF- β family. TGF- β is a protein that comes in three isoforms: TGF- β 1, TGF- β 2 and TGF- β 3. The TGF- β family includes inhibins, activin, anti-müllerian hormone, bone morphogenetic protein, decapentaplegic and Vg-1. TGF- β controls proliferation, differentiation, and other functions of cells. It can also act as a negative autocrine growth factor.

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[0035] FGFs are a family of growth factors involved in wound healing and embryonic development. The FGFs are heparin-binding proteins and interact with cell-surface associated heparan sulfate proteoglycans to assist in FGF signal transduction. FGF stimulates the proliferation of fibroblasts (a connective tissue cell) that give rise to granulation tissue, which fills up a wound space (i.e., the gap in a ruptured tendon) early in the wound healing process.

[0036] PDGF is a dimeric glycoprotein composed of two A or two B chains that regulates cell growth and division. In particular, it plays a role in blood vessel formation (angiogenesis), particularly the growth of blood vessels from already existing blood vessel tissue. Further, PDGF is an element in cellular division for fibroblasts.

[0037] EGF also plays a role in the regulation of cell growth, proliferation and differentiation. EGF acts by binding with high affinity to epidermal growth factor receptors (EGFR) on cell surfaces to stimulate the tyrosine kinase activity of the receptors. The tyrosine kinase activity in turn initiates a signal transduction cascade, which results in a variety of biochemical changes within the cell (e.g., increased intracellular calcium levels, increased glycolysis and protein synthesis, and increased expression of the gene for EGFR) that lead to DNA synthesis and cell proliferation.

[0038] VEGF is a signaling protein involved in angiogenesis. VEGF has been shown to stimulate endothelial cell mitogenesis and cell migration. VEGF is also a vasodilator and increases microvascular permeability.

[0039] Thus, the above growth factors in PRP stimulate cell proliferation, differentiation, and migration at the site of the tendon gap, and stimulate the growth of blood vessels to supply nutrients to the tissue growth at the site of the tendon gap. This further promotes healing of the ruptured tendon.

[0040] Apart from the above growth factors, PRP as the second biocompatible material 24 may also have an additional component or components that aid in cell growth and tissue repair added to it. These may be additional growth factors, such as those listed and discussed above (so that the PRP has an enhanced concentration of its natural growth factors growth factors), or may be additional growth factors that are not inherently present in PRP. Alternatively, the additional component or components may be other than growth factors, for example, components having scaffold properties. In one embodiment, such a component is fibrin. As is known to those of

ordinary skill in the art, fibrin is a protein that is polymerised to form a "mesh" that forms a hemostatic clot (in conjunction with platelets) over a wound site.

[0041] In an alternate embodiment, the second biocompatible material 24 may be a material other than PRP. For example, the second biocompatible material 24 may be a hydrogel. Hydrogels are well known to those skilled in the art, and are a broad class of polymeric materials that swell extensively in water but do not dissolve in water. A hydrogel can be formed by polymerizing a hydrophilic monomer in an aqueous solution under conditions where the polymer becomes cross-linked, thus creating a three dimensional polymer network sufficient to gel the solution. Hydrogels are used extensively in biomaterials and have desirable properties. They can be made nontoxic and compatible with tissue, and they are usually highly permeable to water, ions and small molecules. When used as scaffolds, hydrogels may contain human cells in order to repair tissue. Common ingredients for hydrogels are, for example, polyvinyl alcohol, sodium polyacrylate, acrylate polymers and copolymers with an abundance of hydrophilic groups. Natural hydrogel materials are being investigated for tissue engineering, and include agarose, methylcellulose, hylaronan, and other naturally derived polymers. Such hydrogels that may be used in embodiments of the present invention may have additional components added to them. Such components may include, but are not limited to, growth factors (such as TGF- β , FGF, PDGF, VEGF, and others) and fibrin, as discussed above.

[0042] Thus, the composition of the present invention can bridge a tendon gap 12 without taking or using any autologous tissues. It provides, for example, both a scaffold (the first biocompatible material 10) and growth factors (the second biocompatible material 24) to enhance tissue regeneration.

[0043] Another aspect of the present invention provides a method of repairing a ruptured tendon 16. Fig. 1 depicts a ruptured Achilles tendon 16. The tendon 16 includes a first end 14 and a second end 18. Referring now to Fig. 2, in one embodiment, the method includes positioning a first end 20 of a first biocompatible material 10 adjacent a first end 14 of a ruptured tendon 16, and positioning a second end 22 of the first biocompatible material 10 adjacent a second end 18 of the ruptured tendon 16. Thus, the first biocompatible material 10 provides a scaffold for tendon cell growth and tissue repair. This first biocompatible material 10 may withstand a tensile load of up to 250 N. Positioning the first end 20 and the second end 22 of the first biocompatible

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material 10 may further include anchoring the first end 20 of the first biocompatible material 10 to the first end 14 of the ruptured tendon 16, such as by the use of sutures 26, and anchoring the second end 22 of the first biocompatible material 10 to the second end 18 of the ruptured tendon 16, such as by the use of sutures 26. Those of ordinary skill in the art will recognize that sutures are not the only method of anchoring the first biocompatible material to a tendon, and that other methods suitable for the purposes of the present invention may be used. Such other methods include, but are not limited to, the use of staples and/or tacks.

[0044] Referring to Fig. 3, a second biocompatible material 24 may be positioned between the first and second ends 14,18 of the ruptured tendon 16. The second biocompatible material 24 may include at least one bioactive agent that can stimulate tendon cell growth and tissue repair. In particular, positioning the second biocompatible material 24 between the first and second ends 14,18 of the ruptured tendon 16 may further include positioning the second biocompatible material 24 adjacent the first biocompatible material 10. Further still, and referring now to Fig. 5, positioning the second biocompatible material 24 adjacent the first biocompatible material 10 may include anchoring the second biocompatible material 24 to the first biocompatible material 10, such as by the use of sutures 26. Alternatively or additionally, the method may further include anchoring a first end of the second biocompatible material 24 to the first end 14 of the ruptured tendon 16 and anchoring a second end of the second biocompatible material 24 to the second end 18 of the ruptured tendon 16, such as by the use of sutures 26 (see Fig. 4). Those of ordinary skill in the art will recognize that sutures are not the only method of anchoring the second biocompatible material to the first biocompatible material, or to a tendon, and that other methods suitable for the purposes of the present invention may be used. Such other methods include, but are not limited to, the use of fibrin glue and/or a hydrogel.

[0045] In another embodiment, a method of repairing a ruptured Achilles tendon 16 may include positioning a first end 20 of a biocompatible material adjacent a first end 14 of a ruptured Achilles tendon 16, and positioning a second end 22 of the biocompatible material adjacent a second end 18 of the ruptured Achilles tendon 16. Again, the biocompatible material provides a scaffold for tendon cell growth and tissue repair, and the biocompatible material can withstand, in one particular embodiment, a tensile load up to 250 N. In various embodiments, the first biocompatible material 10 can withstand a minimum load of 150N, can preferably withstand a

tensile load between 150N and 250N, and more preferably can withstand a tensile load of 200N to 250N.

[0046] The method may further include anchoring the first end 20 of the biocompatible material to the first end 14 of the ruptured Achilles tendon 16, and anchoring the second end 22 of the biocompatible material to the second end 18 of the ruptured Achilles tendon 16. Anchoring the first end 20 and the second end 22 of the biocompatible material may particularly include using sutures 26 to anchor the first end 20 of the biocompatible material to the first end 14 of the ruptured Achilles tendon 16, and using sutures 26 to anchor the second end 22 of the biocompatible material to the second end 18 of the ruptured Achilles tendon 16.

[0047] While the invention has been illustrated by the description of various embodiments, and while the various embodiments have been described in considerable detail, the inventors do not intend to restrict or in any way limit the scope of the appended claims to such detail. Additional advantages and modifications will readily appear to those skilled in the art. Moreover, the various features of the invention may be used alone or in numerous combinations depending on the needs and preferences of the user. Therefore, the invention in its broader aspects is not limited to the specific details, representative apparatus and methods, and illustrative examples shown and described. Accordingly, departures may be made from such details without departing from the scope or spirit of the general inventive concept.

Claims:

1. A composition for repairing a connective tissue, comprising:
a first biocompatible material to provide a scaffold for tendon cell growth and tissue repair; and
a second biocompatible material including at least one bioactive agent that can stimulate tendon cell growth and tissue repair.
2. The composition of claim 1, wherein the first biocompatible material is acellular.
3. The composition of claim 2, wherein the first biocompatible material includes collagen and elastin.
4. The composition of claim 3, wherein the first biocompatible material is purified and cross-linked.
5. The composition of claim 1, wherein the first biocompatible material is autogenic, allogenic, xenogenic, or synthetic.
6. The composition of claim 5, wherein the first biocompatible material is xenogenic and comprises porcine dermal tissue.
7. The composition of claim 1, wherein the first biocompatible material can withstand a tensile load up to 250 N.
8. The composition of claim 1, wherein the second biocompatible material is autogenic.
9. The composition of claim 1 wherein the second biocompatible material includes at least one of platelet rich plasma, a collagen-based material, or a hydrogel.
10. The composition of claim 1, wherein the second biocompatible material includes one or more growth factors chosen from TGF- β , FGF, PDGF, EGF, VEGF, and combinations thereof.
11. A composition for bridging a ruptured connective tissue, comprising a biocompatible material to provide a scaffold for tendon cell growth and tissue repair, wherein the biocompatible material can withstand a tensile load up to 250 N.
12. The composition of claim 11, wherein the biocompatible material is acellular.
13. The composition of claim 12, wherein the biocompatible material includes collagen and elastin.
14. The composition of claim 13, wherein the biocompatible material is purified and cross-linked.

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15. The composition of claim 11, wherein the biocompatible material is autogenic, allogenic, xenogenic, or synthetic.
16. The composition of claim 15, wherein the biocompatible material is xenogenic and comprises porcine dermal tissue.
17. The composition of claim 11, wherein the biocompatible material is chosen from allogenic and xenogenic material.
18. The composition of claim 11, further comprising a second biocompatible material including at least one bioactive agent that can stimulate tendon cell growth and tissue repair.
19. The composition of claim 18, wherein the second biocompatible material is autogenic.
20. The composition of claim 18, wherein the second biocompatible material includes at least one of platelet rich plasma, a collagen-based material, or a hydrogel.
21. The composition of claim 18, wherein the second biocompatible material includes one or more growth factors chosen from TGF- β , FGF, PDGF, EGF, VEGF, and combinations thereof.
22. A method of repairing a ruptured connective tissue, the method comprising:
 - positioning a first end of a first biocompatible material adjacent a first end of a ruptured connective tissue;
 - positioning a second end of the first biocompatible material adjacent a second end of the ruptured connective tissue; and
 - positioning a second biocompatible material between the first and second ends of the ruptured connective tissue, wherein the first biocompatible material provides a scaffold for cell growth and tissue repair, and the second biocompatible material includes at least one bioactive agent that can stimulate cell growth and tissue repair.
23. The method of claim 22, wherein positioning the first end and the second end of the first biocompatible material further comprises suturing the first end of the first biocompatible material to the first end of the ruptured connective tissue, and suturing the second end of the first biocompatible material to the second end of the ruptured connective tissue.
24. The method of claim 22, wherein positioning the second biocompatible material between the first and second ends of the ruptured connective tissue further comprises positioning the second biocompatible material adjacent the first biocompatible material.

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25. The method of claim 24, wherein positioning the second biocompatible material adjacent the first biocompatible material further comprises suturing the second biocompatible material to the first biocompatible material.
26. The method of claim 24, further comprising suturing a first end of the second biocompatible material to the first end of the ruptured connective tissue and suturing a second end of the second biocompatible material to the second end of the ruptured connective tissue.
27. The method of claim 22, wherein the connective tissue is chosen from a tendon, a ligament, and a meniscus.
28. A method of repairing a ruptured connective tissue, the method comprising:
positioning a first end of a biocompatible material adjacent a first end of a ruptured connective tissue; and
positioning a second end of the biocompatible material adjacent a second end of the ruptured connective tissue; wherein the biocompatible material provides a scaffold for connective tissue cell growth and tissue repair, and wherein the biocompatible material can withstand a tensile load up to 250 N.
29. The method of claim 28, further comprising anchoring the first end of the biocompatible material to the first end of the ruptured connective tissue, and anchoring the second end of the biocompatible material to the second end of the ruptured connective tissue.
30. The method of claim 29, wherein anchoring the first end and the second end of the biocompatible material comprises suturing the first end of the biocompatible material to the first end of the ruptured connective tissue, and suturing the second end of the biocompatible material to the second end of the ruptured connective tissue.
31. The method of claim 28, further comprising positioning a second biocompatible material between the first and second ends of the ruptured connective tissue, wherein the first biocompatible material provides a scaffold for connective tissue cell growth and tissue repair, and the second biocompatible material includes at least one bioactive agent that can stimulate connective tissue cell growth and tissue repair.
32. The method of claim 31, wherein the second biocompatible material is autogenic.
33. The method of claim 31, wherein the second biocompatible material includes at least one of platelet rich plasma, a collagen-based material, or a hydrogel.

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34. The method of claim 31, wherein the second biocompatible material includes one or more growth factors chosen from TGF- β , FGF, PDGF, EGF, VEGF, and combinations thereof.
35. The method of claim 28, wherein the connective tissue is chosen from a tendon, a ligament, and a meniscus.

