

(19) World Intellectual Property Organization
International Bureau(43) International Publication Date
2 March 2006 (02.03.2006)

PCT

(10) International Publication Number
WO 2006/023725 A2(51) International Patent Classification⁷: G01N 21/64,
A61B 5/00, G01N 21/77(74) Agent: RENZONI, George, E.; Christensen O'Connor
Johnson Kindness PLLC, 1420 Fifth Avenue, Suite 2800,
Seattle, WA 98101 (US).(21) International Application Number:
PCT/US2005/029559(81) Designated States (unless otherwise indicated, for every
kind of national protection available): AE, AG, AL, AM,
AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN,
CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI,
GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE,
KG, KM, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA,
MD, MG, MK, MN, MW, MX, MZ, NA, NG, NI, NO, NZ,
OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL,
SM, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC,
VN, YU, ZA, ZM, ZW.

(22) International Filing Date: 19 August 2005 (19.08.2005)

(84) Designated States (unless otherwise indicated, for every
kind of regional protection available): ARIPO (BW, GH,
GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM,
ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM),
European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI,
FR, GB, GR, HU, IE, IS, IT, LT, LU, LV, MC, NL, PL, PT,
RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA,
GN, GQ, GW, ML, MR, NE, SN, TD, TG).

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:
60/602,684 19 August 2004 (19.08.2004) US
60/674,393 22 April 2005 (22.04.2005) US(71) Applicant (for all designated States except US): BLOOD
CELL STORAGE, INC [US/US]; Suite 3800, 999 Third
Avenue, Seattle, WA 98104 (US).

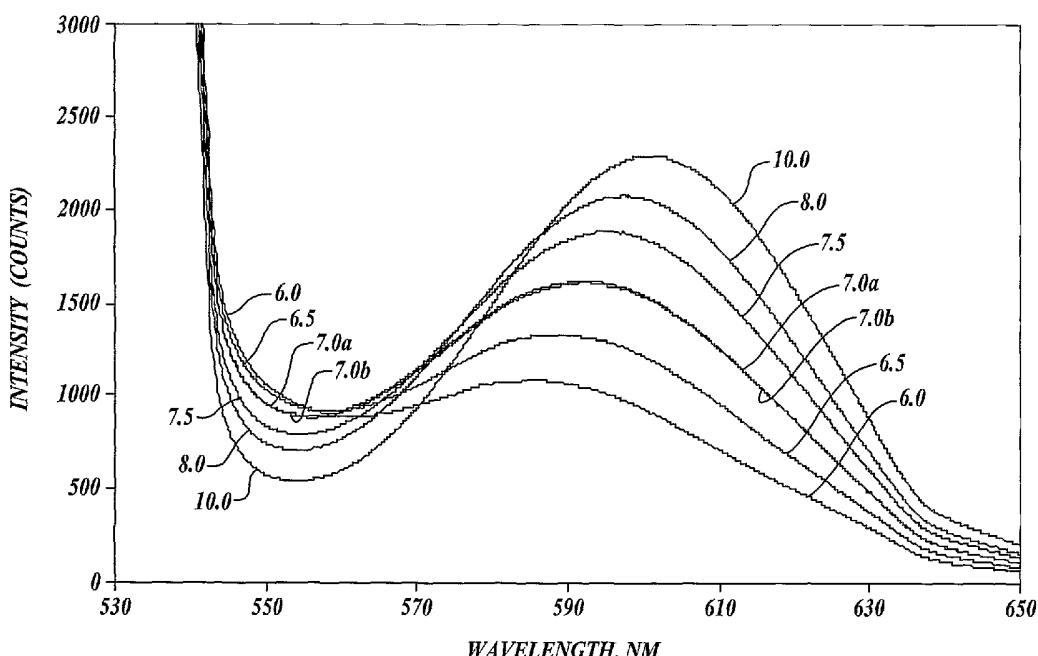
(72) Inventors; and

(75) Inventors/Applicants (for US only): REED, Michael, W.
[US/US]; 3575 NE 180th Street, Lake Forest Park, WA
98155 (US). GEELHOOD, Steven, J. [US/US]; 315 NW
86th Street, Seattle, WA 98117 (US). HARRIS, Paul, C.
[US/US]; 3022 - 184th Place SE, Bothell, WA 98012 (US).
PFALZGRAF, Randy, D. [US/US]; 18420 - 126th Street
SE, Snohomish, WA 98290 (US).

Published:

— without international search report and to be republished
upon receipt of that reportFor two-letter codes and other abbreviations, refer to the "Guid-
ance Notes on Codes and Abbreviations" appearing at the begin-
ning of each regular issue of the PCT Gazette.

(54) Title: FLUORESCENT pH DETECTOR SYSTEM AND RELATED METHODS



WO 2006/023725 A2

(57) Abstract: Fluorescent pH detector and methods for measuring pH using the fluorescent ph detector.

FLUORESCENT pH DETECTOR SYSTEM AND RELATED METHODS

FIELD OF THE INVENTION

The present invention relates to a fluorescent pH detector and methods for measuring
5 pH using the fluorescent pH detector.

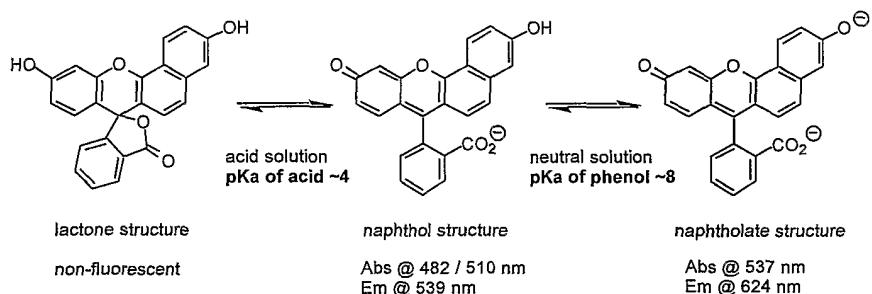
BACKGROUND OF THE INVENTION

Optical sensors (optrodes) for measuring pH are well known. Certain aromatic organic compounds (like phenolphthalein) change color with pH and can be immobilized on solid supports to form "pH paper." These visual indicators are easy to use, but do not
10 provide a quantitative reading. The color changes can be difficult to distinguish accurately, and can be masked by colored analyte. Fluorescent indicators have also been used as optical sensors. pH Sensitive fluorescent dyes can be immobilized on solid supports and generally are more sensitive in comparison to the simple color changing (absorbance or reflectance based) indicators. The improved sensitivity of fluorescent
15 indicators allows the solid support to be miniaturized, and this has been used to advantage in development of fiber optic sensor devices for measuring pH, CO₂, and O₂ parameters in blood.

A specific need in the medical industry exists for accurate pH measurement of blood. The pH of blood, or other bodily fluids (pleural effusions) can be associated with
20 certain physiologic responses associated with pathology. Blood gas analyzers are common critical care instruments. Depending on storage conditions, the pH of separated blood components (plasma, platelets) can change rapidly due to off-gassing of dissolved CO₂ from the enriched venous blood that is collected from a donor. Platelets in particular are metabolically active, and generate lactic acid during storage at 20-22°C. European
25 quality guidelines for platelets prepared by the "buffycoat method" require pH of stored platelets to be pH 6.8-7.4 at 37°C (7.0-7.6 at 22°C).

Seminaphthofluorescein (SNAFL) compounds and the related seminaphthorhodafluor (SNARF) compounds are commercially available ratiometric fluors (Molecular Probes, Inc., Eugene, OR; see, for example, U.S. Patent No. 4,945,171) and their synthesis and spectral properties have been described. These compounds have
30 advantages including long wavelength absorbance that can be efficiently excited with

LED light sources. Relevant acid/base equilibria and associated spectral properties are shown below.



5

Deiprotonation of the naphthol structure of SNAFL dyes gives a naphtholate molecule with longer wavelength fluorescence emission. The pKa is the pH value where the two molecular species form in equal amounts. SNAFL compounds with reactive linker groups that allow their conjugation to other molecules of interest are also commercially 10 available.

Various methods have been used to immobilize "ratiometric" dyes to solid supports for use in fiber optic pH detectors. Carboxynaphthofluorescein (CNF) has been conjugated to aminoethyl-cellulose and this material was glued to polyester (Mylar) films to make sensing membranes for optrodes. The pKa of this material was 7.41, slightly 15 lower than the free CNF (pKa 7.62). The use of tetraethoxysilane to trap CNF in a sol-gel glass that was formed on glass cover slips has also been reported. The pKa of this material was 7.46. A 9-chloro substituted SNAFL analog (SNAFL-2) has been reacted with polyvinylamine and the residual amino groups were crosslinked with a photocrosslinker to form a gel-like coating on acrylic fibers. The pKa of this fiber-optic 20 sensor was 7.14, significantly lower than the published pKa of the free SNAFL compound (pKa ~7.7). This shows that molecular environment and linker structure surrounding the immobilized dye can alter the performance of a pH detector.

Despite the advances made in the detection of pH noted above, there exists a need for improved methods and devices for measuring pH. The present invention seeks to 25 fulfill this need and provides further related advantages.

SUMMARY OF THE INVENTION

In one aspect, the present invention provides a method for measuring the pH of a sample. The method is useful in measuring the pH of blood and blood products. In one

embodiment, the method is useful in measuring the pH of blood or blood products sealed in a vessel. In one embodiment, the method includes the steps of:

- (a) irradiating a fluorescent species immobilized on a substrate with excitation light emanating from a probe physically isolated from the fluorescent species immobilized on the substrate, wherein the fluorescent species immobilized on the substrate is in liquid communication with a sample, wherein the excitation light has a wavelength sufficient to effect fluorescent emission from the fluorescent species, wherein the fluorescent species exhibits a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength, the ratio of the first and second emission intensities being dependent on pH; and
- 5 (b) measuring the first and second emission intensities to determined the pH of the sample.

In the method, the probe is physically isolated from the fluorescent species immobilized on the substrate. As used herein, the term "physically isolated" refers to the physical isolation of the probe from the sample being interrogated. The probe providing excitation light and receiving emission light does contact the sample being interrogated. In the method of the invention, the sample is in contact (i.e., liquid communication) with the substrate-immobilized fluorescent species. The probe is isolated from and does not come not physical contact with the sample. The isolation of the probe from the sample is 10 illustrated in FIGURES 3 and 5. In one embodiment, the probe is isolated from the fluorescent species by a window transparent to the excitation light and the fluorescent emission.

In one embodiment, the probe comprises one or more optical fibers.

In the method, the fluorescent species is a ratiometric fluorescent species. In one embodiment, the fluorescent species is selected from a naphthofluorescein compound and a seminaphthorhodamine compound. In one embodiment, the naphthofluorescein compound is selected from a seminaphthofluorescein compound and a carboxynaphthofluorescein compound. In one embodiment, the seminaphthofluorescein compound is selected from 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-25 benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one (also referred to herein as "SNAFL-1", see FIGURE 7A) and 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthene-7-yl)benzoic acid (also referred to herein as "EBIO-3", see FIGURE 7E).

In one embodiment, the fluorescent species immobilized on a substrate comprises a conjugate of a fluorescent species and a macromolecule. In one embodiment, the macromolecule is an albumin. In one embodiment, the macromolecule is a serum albumin. In one embodiment, the macromolecule is a human serum albumin. In one embodiment, the macromolecule is a recombinant human serum albumin. In one embodiment, the fluorescent species immobilized on a substrate comprises a naphthofluorescein/serum albumin conjugate. In one embodiment, the fluorescent species immobilized on a substrate comprises a seminaphthofluorescein/human serum albumin conjugate.

As noted above, the method is suitable for measuring the pH of blood or blood products sealed in a vessel. In one embodiment, the fluorescent species immobilized on a substrate is introduced into a sealed vessel by a means that preserves the vessel's seal.

In another aspect of the invention, a system for measuring pH is provided. In one embodiment, the system includes

- (a) a light source for exciting a fluorescent species, wherein the fluorescent species has a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength;
- (b) a first emission detector for measuring the first emission intensity;
- (c) a second emission detector for measuring the second emission intensity;
- (d) an excitation lightguide for transmitting excitation light from the light source to the fluorescent species, wherein the lightguide comprises a first terminus proximate to the light source and a second terminus distal to the light source;
- (e) a first emission lightguide for transmitting emission from the fluorescent species to the first emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;
- (f) a second emission lightguide for transmitting emission from the fluorescent species to the second emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;
- (g) a probe housing the distal termini of the excitation lightguide, first emission lightguide, and second emission light guide; and
- (h) an assembly for receiving the probe, the assembly comprising:

(i) a housing for receiving the probe, wherein the housing is adapted for receiving the probe at a first end and terminating with a window at the second end, the window being transparent to the excitation and the emission light,

5 (ii) a tip member reversibly connectable to the housing's second end, wherein the tip member is adapted to receive liquid from a sample to be measured, and

(iii) a fluorescent species immobilized on a substrate intermediate the tip member and the window, wherein the fluorescent species immobilized on the substrate is in liquid communication with the sample during the measurement, and wherein the window physically isolates the probe member from the fluorescent species

10 immobilized on the substrate.

In one embodiment, the light source is a light-emitting diode.

In one embodiment, the first and second detectors are photodiodes.

In one embodiment, the excitation lightguide, the first emission lightguide, and the second emission lightguide are optical fibers.

15 In one embodiment, the housing comprises a tapered tube terminating with the window.

In one embodiment, the tip member comprises a spike for puncturing a sealed vessel.

20 The fluorescent species useful in the system include those noted above in regard to the method and described in further detail below. In one embodiment, the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

25 In a further aspect, the invention provides an assembly useful for introducing a fluorescent species immobilized on a substrate into a sample. The assembly is particularly useful for introducing a fluorescent species immobilized on a substrate into a sample sealed in a vessel. In one embodiment, the assembly includes

(a) a housing having a first open end and a second closed end, wherein the closed end comprises a window transparent to visible light;

(b) a tip member reversibly connectable to the housing closed end, wherein the tip member is adapted to expose the housing window; and

30 (c) a fluorescent species immobilized on a substrate intermediate the housing window and tip member.

The tip member is adapted to expose the housing window. By exposing the housing window to the environment exterior to the tip member, the fluorescent species

immobilized on the substrate intermediate the housing window and tip member is in liquid communication with the sample to be measured.

5 In one embodiment, the housing is tapered. In one embodiment, the tip member comprises a spike for puncturing a sealed vessel. The fluorescent species useful in the assembly include those noted above in regard to the method and described in further detail below. In one embodiment, the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

In another aspect, the invention provides a blood bag or blood product bag that includes the assembly described above.

10 In a further aspect of the invention, an environment-sensitive fluorophore protein conjugate is provided. In one embodiment, the conjugate includes an environment-sensitive fluorophore covalently coupled to an albumin. In one embodiment, the environment-sensitive fluorophore is a pH-sensitive fluorophore, an oxygen-sensitive fluorophore, a nucleic acid-sensitive fluorophore, an ion-sensitive fluorophore, a 15 glucose-sensitive fluorophore, a lipid-sensitive fluorophore, or an enzyme-sensitive fluorophore.

In one embodiment, the environment-sensitive fluorophore is a pH-sensitive fluorophore selected from a naphthofluorescein compound and a seminaphthorhodamine compound. In one embodiment, the naphthofluorescein compound is a 20 seminaphthofluorescein compound or a carboxynaphthofluorescein compound. In one embodiment, the seminaphthofluorescein compound is 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one or 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthen-7-yl)benzoic acid.

25 In one embodiment, the albumin is a serum albumin. In one embodiment, the albumin is a human serum albumin. In one embodiment, the albumin is a recombinant human serum albumin.

In one embodiment, the environment-sensitive fluorophore is 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthen-7-yl)benzoic acid and the albumin is human serum albumin.

30 It will be appreciated that the method and system of the invention described above can be modified to include a particular environment-sensitive fluorophores to provide methods and systems specific to the utility provided by the particular fluorophore.

In another aspect, the invention provides a substrate-immobilized fluorescent species. In one embodiment, the substrate-immobilized fluorescent species is a membrane-immobilized fluorescent species. In one embodiment, the membrane-immobilized fluorescent species is a conjugate of a naphthofluorescein compound and an albumin adhered to a membrane. In one embodiment, the membrane is a microporous membrane. In one embodiment, the membrane is a nitrocellulose membrane, a membrane of mixed esters of nitrocellulose and cellulose acetate, a polyethylene terephthalate membrane, a polycarbonate membrane, and a polyimide membrane.

In one embodiment, the naphthofluorescein compound is a 10 seminaphthofluorescein compound or a carboxynaphthofluorescein compound. In one embodiment, the naphthofluorescein compound is 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one or 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthen-7-yl)benzoic acid.

In one embodiment, the albumin is a serum albumin. In one embodiment, the albumin is a human serum albumin. In one embodiment, the albumin is a recombinant human serum albumin.

In another aspect of the invention, a method for measuring carbon dioxide is provided. In one embodiment, the method includes the steps of:

(a) irradiating a fluorescent species immobilized on a substrate with excitation light emanating from a probe physically isolated from the fluorescent species immobilized on the substrate, wherein the fluorescent species immobilized on the substrate is in liquid communication with a solution having pH responsiveness to carbon dioxide present in a liquid sample, wherein the solution having pH responsiveness to carbon dioxide is in communication with the liquid sample through a selectively 20 permeable membrane, wherein the excitation light has a wavelength sufficient to effect fluorescent emission from the fluorescent species, wherein the fluorescent species exhibits a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength, the ratio of the first and second emission intensities being dependent on pH;

(b) measuring the first and second emission intensities to determined the pH of the solution having pH responsiveness; and

(c) correlating the pH of the solution having pH responsiveness to the carbon dioxide level in the sample.

In one embodiment, the probe is physically isolated from the fluorescent species immobilized on the substrate by a window transparent to the excitation light and the fluorescent emission. In one embodiment, the probe comprises one or more optical fibers.

5 In one embodiment, the sample comprises blood or a blood product. In one embodiment, the sample is contained within a sealed vessel. In one embodiment, the fluorescent species immobilized on a substrate is introduced into a sealed vessel by a means that preserves the vessel's seal.

10 The fluorescent species useful in the method include those noted above in regard to the method for measuring pH and described in further detail below. In one embodiment, the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

15 In another aspect, the invention provides a system for measuring carbon dioxide. The system is useful for measuring the carbon dioxide level in a liquid sample. In one embodiment, the system includes:

(a) a light source for exciting a fluorescent species, wherein the fluorescent species has a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength;

20 (b) a first emission detector for measuring the first emission intensity;

(c) a second emission detector for measuring the second emission intensity;

(d) an excitation lightguide for transmitting excitation light from the light source to the fluorescent species, wherein the lightguide comprises a first terminus proximate to the light source and a second terminus distal to the light source;

25 (e) a first emission lightguide for transmitting emission from the fluorescent species to the first emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;

(f) a second emission lightguide for transmitting emission from the fluorescent species to the second emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;

30 (g) a probe housing the distal termini of the excitation lightguide, first emission lightguide, and second emission light guide; and

(h) an assembly for receiving the probe, the assembly comprising:

(i) a housing for receiving the probe, wherein the housing is adapted for receiving the probe at a first end and terminating with a window at the second end, the window being transparent to the excitation and the emission light,

5 (ii) a tip member reversibly connectable to the housing's second end, wherein the tip member comprises a chamber for receiving a solution having pH responsiveness to carbon dioxide present in a liquid sample, wherein the solution having pH responsiveness to carbon dioxide is in liquid communication with the liquid sample through a selectively permeable membrane, and

10 (iii) a fluorescent species immobilized on a substrate intermediate the tip member and the window, wherein the fluorescent species immobilized on the substrate is in liquid communication with the solution having pH responsiveness to carbon dioxide during the measurement, and wherein the window physically isolates the probe member from the fluorescent species immobilized on the substrate.

In one embodiment, the light source is a light-emitting diode.

15 In one embodiment, the first and second detectors are photodiodes.

In one embodiment, the excitation lightguide, the first emission lightguide, and the second emission lightguide are optical fibers.

In one embodiment, the housing comprises a tapered tube terminating with the window.

20 In one embodiment, the selectively permeable membrane is permeable to carbon dioxide.

In one embodiment, the tip member comprises a spike for puncturing a sealed vessel.

The fluorescent species useful in the method include those noted above in regard

25 to the method for measuring pH and described in further detail below. In one embodiment, the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing aspects and many of the attendant advantages of this invention will

30 become more readily appreciated as the same become better understood by reference to the following detailed description, when taken in conjunction with the accompanying drawings, wherein:

FIGURE 1A is a schematic illustration of a representative system of the invention for measuring pH;

FIGURE 1B is a schematic illustration of an optical platform useful in the system of the invention for measuring pH;

5 FIGURE 2 is a schematic illustration of a representative housing for excitation and emission light guides useful in the system of the invention;

FIGURE 3 illustrates the relationship between the excitation/emission optical fiber housing and the sealed vessel port;

10 FIGURES 4A-4C illustrate a representative port assembly for introducing a substrate-immobilized fluorescent species into a sealed vessel, FIGURE 4A illustrates the assembled port, FIGURE 4B is an exploded view of the port assembly; and FIGURE 4C is a plan view of tip;

15 FIGURES 5A and 5B illustrate representative sealed vessels incorporating the substrate-immobilized fluorescent species, FIGURE 5A shows a sealed vessel in which substrate was introduced through process of puncture and reseal, FIGURE 5B shows a sealed vessel incorporating substrate during vessel manufacture;

FIGURE 6 is a representative port assembly useful in the manufacture of a sealed vessel;

20 FIGURES 7A-E illustrate the structures of representative seminaphthofluorescein compounds useful in the method and system of the invention;

FIGURE 8 illustrates the emission spectra as a function of pH of a representative fluorescent species (SNAFL-1) useful in the method and system of the invention;

FIGURE 9 illustrates the emission spectra as a function of pH of a representative fluorescent species (EBIO-3) useful in the method and system of the invention;

25 FIGURE 10 is a schematic illustration of the preparation of a representative fluorophore-protein (EBIO-3/HSA) conjugate useful in the method and system of the invention;

30 FIGURE 11 illustrates the emission spectra as a function of pH of a representative fluorophore-protein conjugate (SNAFL-1/HSA) useful in the method and system of the invention;

FIGURE 12 illustrates the emission spectra as a function of pH of a representative fluorophore-protein conjugate (EBIO-3/HSA) useful in the method and system of the invention;

FIGURE 13 illustrates the emission spectra of a representative substrate-immobilized fluorophore-protein conjugate (SNAFL-1/HSA) as a function of pH (Oxyphen);

5 FIGURE 14 illustrates the emission spectra of a representative substrate-immobilized fluorophore-protein conjugate (SNAFL-1/HSA) as a function of pH (nitrocellulose);

FIGURE 15 illustrates the emission spectra of a representative substrate-immobilized fluorophore-protein conjugate (EBIO-3/HSA) as a function of pH (nitrocellulose);

10 FIGURE 16 illustrates the data used in the method of the invention for measuring pH;

FIGURE 17 illustrates the results of the method of the invention for platelet rich plasma;

15 FIGURE 18 illustrates the correlation of pH results for platelet rich plasma obtained by the method and system of the invention;

FIGURE 19 illustrates stability of a representative substrate-immobilized fluorophore conjugate of the invention;

FIGURE 20 illustrates a representative device of the invention for measuring carbon dioxide in a sealed vessel;

20 FIGURE 21 illustrates the effect of probe position on fluorescent intensity in measuring pH in accordance with the invention; and

FIGURE 22 illustrates the effect of membrane pore size on fluorescent intensity in measuring pH in accordance with the invention.

DETAILED DESCRIPTION OF THE INVENTION

25 The present invention provides a method for measuring pH and a system for measuring pH. The method and system are suited to measure the pH of a specimen contained in a sealed container.

30 In one aspect of the invention, a method for measuring pH is provided. In the method, pH is determined by comparing fluorescent emission intensities from a single fluorescent species having pH-dependent fluorescent emission. The fluorescent species having pH-dependent fluorescent emission has a first emission intensity at a first wavelength and a second emission intensity at a second wavelength, the first and second emission intensities being characteristic of pH in the environment of the fluorescent

species. The ratio of the first and second emission intensities provides pH measurement. Calibration of the first and second emission intensities provides an intensity-based reference (ratio information) that is used to determine the pH of the environment of the fluorescent species.

5 The method of the invention is a fluorescent wavelength-ratiometric method. As used herein, the term "fluorescent wavelength-ratiometric" refers to the method by which the first and second fluorescent emission intensities measured at first and second emission wavelengths, respectively, are ratioed to provide pH information.

10 In the method, the fluorescent species having pH-dependent fluorescent emission is immobilized on a substrate in contact with the sample such that the fluorescent species is in contact with the sample. The immobilized fluorescent species in contact with the sample is located in the sample such that the fluorescent species can be interrogated. The fluorescence measurement is made by irradiating the fluorescent species at a wavelength sufficient to elicit fluorescent emission, which is then measured. Because of the 15 pH-dependent nature of the fluorescent species' emission profile (i.e., first and second fluorescent emission intensities measured at first and second emission wavelengths, respectively) the measurement of the fluorescent emission profile yields the pH of the fluorescent species' environment (i.e., sample pH).

20 In one embodiment of the method of the invention, the sample for which the pH is to be determined is contained in a sealed vessel. This method is suitable for measuring pH of blood and blood products sealed in a conventional blood storage vessel.

25 In another embodiment, the sample for which the pH is to be determined is contained in an open vessel. As used herein, the term "open vessel" refers to a vessel that is not sealed. This method is suitable where contamination of the sample being measured is to be avoided. In this method, the probe is cleaned and/or sterilized and is used once and discarded. This method is suitable for measuring the pH of materials used in food, pharmaceutical, or biological research where the vessel containing the material is not sealed (i.e., open). Such a "lab-use" system includes a tip (see description below) placed onto the probe. The pH measurement is made by immersing the tip into the sample and 30 measuring pH. The tip is removed from the sample, removed from the probe, and discarded.

In the method for measuring the pH of a contained sample, the substrate-immobilized fluorescent species is introduced into the vessel either before or

after the sample is placed in the vessel. As used herein, the term "sealed vessel" refers to a vessel that prevents its contents from exposure to the environment exterior to the vessel. The sealed vessel prevents the contents of the vessel from contact from, for example, liquids and gases outside of the vessel. The sealed vessel also prevents the contents of 5 the vessel from escaping the vessel.

The vessel can be manufactured to include the substrate-immobilized fluorescent species as a component of the vessel. In such an embodiment, the substrate-immobilized fluorescent species is incorporated into the vessel during manufacture to provide a vessel into which a sample can be later introduced and its pH measured. The manufacture of a 10 vessel incorporating the substrate-immobilized fluorescent species is described in Example 1.

Alternatively, the substrate-immobilized fluorescent species can be introduced into the vessel after the sample has been introduced into the vessel. In such an embodiment, the substrate-immobilized fluorescent species is introduced into the vessel 15 by a process in which the vessel is first punctured (or spiked) to introduce the substrate-immobilized fluorescent species and then resealed to provide a sealed vessel including the sample now in contact with the substrate-immobilized fluorescent species. The process for introducing the substrate-immobilized fluorescent species into a sealed vessel is described in Example 2.

20 As noted above, the vessel including the substrate-immobilized fluorescent species in contact with the sample is sealed before, during, and after interrogation. Interrogation of the fluorescent species requires excitation of the species at a wavelength sufficient to effect fluorescent emission from the species and measurement of that fluorescent emission. In the method of the invention, interrogation is accomplished 25 through a window in the sealed vessel. The fluorescent species is excited by irradiation through the window, and emission from the fluorescent species is collected from the fluorescent species through the window. The window is a component of the sealed vessel and allows for interrogation of the fluorescent species in contact with the sample. The window is sufficiently transparent at the excitation and emission wavelengths to permit 30 interrogation by the method. The substrate-immobilized fluorescent species is positioned in proximity to the window sufficient for interrogation: proximity sufficient to effectively excite the fluorescent species and to effectively collect emission from the fluorescent species. It will be appreciated that for epifluorescence applications, a single

window is used. However, other methods and devices of the invention can include other optical paths, such as straight-through or right angle optical paths, where more than one window can be used.

The method of the invention includes irradiating the substrate-immobilized 5 fluorescent species, which in one embodiment is contained along with a sample in a sealed vessel, at a wavelength sufficient to effect emission from the fluorescent species and to measure that emission. Exciting light and fluorescent emission pass through the sealed vessel's window. In one embodiment, the sealed vessel further includes a port for receiving a housing that holds the excitation light guide and emission light guide. In one 10 embodiment, the excitation light guide includes one or more optical fibers that transmit the excitation light from a light source to the fluorescent species. In one embodiment, the emission light guide includes one or more optical fibers that transmit the emission light from the fluorescent species to a light detector. The port receiving the housing is positioned in proximity to the window sufficient for interrogation: proximity sufficient to 15 effectively excite the fluorescent species and to effectively collect emission from the fluorescent species.

As with all optical fluorescent methods, the method of the invention includes a light source for exciting the fluorescent species and a detector for measuring the emission 20 of the fluorescent species. Light sources, wavelength selection filters, and detectors are selected based on the absorbance and emission profiles of the fluorescent species used in the method.

Suitable light sources provide excitation energy at a wavelength and intensity 25 sufficient to effect fluorescent emission from the fluorescent species. The light source can provide relatively broad wavelength band excitation (e.g., ultraviolet or white light sources) or relatively narrower wavelength band excitation (e.g., laser or light-emitting diode). To enhance excitation efficiency and emission measurement, relatively broad wavelength band exciting light from the source can be selected and narrowed through the use of diffraction gratings, monochromators, or filters to suit the fluorescent species. Suitable light sources include tungsten lamps, halogen lamps, xenon lamps, arc lamps, 30 LEDs, hollow cathode lamps, and lasers.

Suitable detectors detect the intensity of fluorescent emission over the emission wavelength band of the fluorescent species. To enhance emission measurement, fluorescent emission from the fluorescent species source can be selected and narrowed

through the use of diffraction gratings, monochromators, or filters to suit the fluorescent species. Suitable detectors include photomultiplier tubes and solid state detectors, such as photodiodes, responsive to the wavelength emission band of the fluorescent species. Other suitable detectors are photovoltaic cells, PIN diodes, and avalanche photodiodes.

5 Through the use of filters, all of the excitation light that reflects off the target is filtered out before reaching the detector. This can be achieved by using filters in both the excitation and emission optical paths. In certain instances, reflected excitation light (which is many orders of magnitude more intense than the emission light) that reaches the detector can swamp the specific signal. Generally, 10E5 (10^5) or greater out-of-band rejection is appropriate in each of the filter sets. Reduction of excitation light can also be achieved by using an angled window so that reflected light is directed away from the emission detector. However, such an optical path is not as effective as filter sets.

10 Excitation light from the source can be directed to the fluorescent species through the use of a light guide, such as one or more optical fibers. Similarly, emission from the fluorescent species can be directed to the detector through the use of a light guide, such as one or more optical fibers.

15 A representative system for carrying out the method of the invention is illustrated schematically in FIGURE 1A. Referring to FIGURE 1A, system 100 includes controller 110 that controls and operates the system components. System components include keypad 120 for inputting information including system commands; display 130 for determining the status of the system and viewing pH determination results; barcode reader 140 for inputting information to the system including the identification of the sample, the pH of which is to be measured by the system; printer 150 for printing system status and pH determination results; battery (or wall plug and power adapter) 160 for 20 powering the system; memory device 165 for storing test results and calibration data; signal processing electronics 170 for commanding the optical platform components and processing signals from the optical platform; and optical platform 180 including an excitation source, emission detectors, light guides, and associated lenses and filters. Optical platform includes probe member 185 housing one or more excitation light guides 25 and two or more emission light guides. FIGURE 1A also illustrates sealed vessel 500 including port 205 for receiving probe member 185.

30 FIGURE 1B is a schematic illustration of an optical platform useful in the system of the invention for measuring pH. Referring to FIGURE 1B, optical platform 180

includes excitation optics 280, first emission optics 380, and second emission optics 480. Excitation optics 280 include light source 282, collimating lens 284, filter 286, focusing lens 288, and excitation light waveguide 290. First emission optics 380 include detector 382, focusing lens 384, filter 386, collimating lens 388, and first emission light waveguide 390. Second emission optics 480 includes detector 482, focusing lens 484, filter 486, collimating lens 488, and second emission light waveguide 490. Excitation light guide 290, first emission light waveguide 390, and second emission light waveguide 490 are housed in probe member 185.

The system's light source is effective in exciting the fluorescent species. Suitable light sources include light-emitting diodes, lasers, tungsten lamps, halogen lamps, xenon lamps, arc lamps, and hollow cathode lamps. In one embodiment, the light source is a light-emitting diode emitting light in the range from 500 to 560 nm. A representative light-emitting diode useful in the system of the invention is a green ultrabright Cotco 503 series LED commercially available from Marktech, Latham NY.

The collimating lens directs light (e.g., excitation light from the light source or first and second emission light from the emission light waveguides) to the bandpass filter. Suitable collimating lenses include Biconvex glass lenses and Plano-convex glass lenses. Representative collimating lenses useful in the system of the invention are the Tech Spec PCX lenses commercially available from Edmund Optics, Barrington, NJ. The excitation collimating lens is 12x36 (diameter by effective focal length in mm) and the first and second emission collimating lenses are 12x18.

The focusing lens focuses light from the bandpass filter to the excitation light waveguide or from the bandpass filter to the detector. Suitable focusing lenses include Biconvex glass lenses and Plano-convex glass lenses. Representative focusing lenses useful in the system of the invention are the Tech Spec PCX lenses commercially available from Edmund Optics, Barrington, NJ. The excitation focusing lens is 12x18 and the first and second emission focusing lenses are 12x15.

Filters are used in the optical platform to narrow the bandwidth of transmitted light.

Suitable excitation filters include bandpass filters, shortpass filters, longpass filters, or a combination of short and long pass filters. In one embodiment, the system uses a shortpass filter that passes light in the range from about 370 nm to 540 nm. A

representative excitation shortpass filter useful in the system of the invention is 540ASP commercially available from Omega Optical, Brattleboro, VT.

Suitable first emission filters include bandpass, shortpass, longpass, or a combination of short and longpass filters. In one embodiment, the bandpass filter passes 5 light in the range from about 595 to 605 nm and has a full width at half height of 10 nm. A representative first emission bandpass filter useful in the system of the invention is 600DF10 commercially available from Omega Optical, Brattleboro, VT.

Suitable second emission filters include bandpass, shortpass, longpass, or a combination of short and longpass filters. In one embodiment, the bandpass filter passes 10 light in the range from about 562 to 573 nm and has a full width at half height of 10 nm. A representative second emission bandpass filter useful in the system of the invention is 568DF10 commercially available from Omega Optical, Brattleboro, VT.

The excitation light waveguide transmits excitation light from the light source through the probe member to the fluorescent species. In one embodiment, the excitation 15 light waveguide includes one or more optical fibers. In one embodiment, the excitation waveguide is a single optical fiber. A representative fiber optic useful in the system of invention is RO2-534 commercially available from Edmund Optics, Barrington, NJ.

The first and second emission light waveguides transmit fluorescent emission from the fluorescent species through the probe member to the first and second emission 20 detectors, respectively.

In one embodiment, the first emission light waveguide includes one or more optical fibers. In one embodiment, the first emission light waveguide includes a plurality of optical fibers. In one embodiment, the first emission light waveguide includes four optical fibers. A representative fiber optic useful in the system of invention is RO2-533 25 commercially available from Edmund Optics, Barrington, NJ.

In one embodiment, the second emission light waveguide includes one or more optical fibers. In one embodiment, the second emission light waveguide includes a plurality of optical fibers. In one embodiment, the second emission light waveguide includes four optical fibers. A representative fiber optic useful in the system of invention 30 is RO2-533 commercially available from Edmund Optics, Barrington, NJ.

Suitable optical fibers useful in the system of the invention include glass or plastic optical fibers from 0.2 to 2 mm diameter.

The system's first and second emission detectors are effective in measuring the first and second fluorescent emissions from the fluorescent species. Suitable detectors include photodiodes, PIN diodes, and photomultiplier tubes. In one embodiment, the first and second emission detectors are photodiodes responsive in the range from 400 to 5 800 nm. Representative photodiodes useful in the system of the invention include BPW34 commercially available from Vishay Intertechnology, Malvern, PA.

A representative probe member housing excitation and emission light guides useful in the system of the invention is illustrated schematically in FIGURE 2. As shown in FIGURE 2, the light guides are optical fibers. Referring to FIGURE 2, probe member 10 185 houses excitation light guide 290, a plurality of first emission light guides 390, and a plurality of second emission light guides 490. In the representative probe member shown in FIGURE 2, there are four first emission light guides 390, and four second emission light guides 490. The four first emission light guides can be considered to be a first channel (e.g., measuring the first fluorescent emission from the fluorescent species) and 15 the four second emission light guides can be considered to be a second channel (e.g., measuring the second fluorescent emission from the fluorescent species). In the illustrated representative probe member, the fibers from each of the two sets of fibers alternate (i.e., alternating fibers 390 and 490) around the central fiber (290). This configuration provides for evening out of "hot spots" so that light collected by the first set 20 is similar to the light collected by the second set.

The relationship between the probe member housing the excitation/emission light guides and the sealed vessel port is illustrated schematically in FIGURE 3. Referring to FIGURE 3, probe member 185 is received by port 205. Port 205 includes window 210, which is transparent to excitation and emission wavelengths used in the fluorescent 25 measurement. Excitation light emanating from light guide 290 passes through window 210 and interrogates substrate 220 on which the fluorescent species is immobilized and which, in the operation of the method of the invention, is in contact with the sample contained in sealed vessel 200. Irradiation of substrate 220 results in excitation of the substrate-immobilized fluorescent species and fluorescent emission from the fluorescent 30 species. Emission from the fluorescent species is received by and transmitted through light guides 390 and 490 to detectors 382 and 482, respectively (see FIGURE 1B). As noted above, the fluorescent species' first emission intensity and the second emission intensity will depend on the pH of the sample.

A representative port assembly for introducing the substrate-immobilized fluorescent species into a sealed vessel is illustrated in FIGURES 4A and 4B. FIGURE 4A illustrates the assembled port and FIGURE 4B is an exploded view of the port assembly.

5 Referring to FIGURES 4A and 4B, port assembly 202 includes port 205 and tip 215. Port 205 is a cylinder terminating with window 210 and having opening 212 for receiving probe member 185 (not shown). In one embodiment, port 205 tapers from opening 212 to window 210 such that the depth of insertion of probe member 185 into port 205 is predetermined by the probe's diameter. In one embodiment, the depth of
10 travel of 185 in assembly 202 is limited by a ledge (not shown). In one embodiment, the optimal distance between probe and membrane was determined to be 2 mm or less. FIGURE 21 illustrates the fluorescence intensity measured as a function of distance between the probe and membrane. When inserted in the port, the face of probe member 185 and window 210 are substantially parallel. Port 205 and tip 215 are adapted such that
15 the port and tip are reversibly connectable. In one embodiment, port 205 includes annular inset 214 and tip 215 includes opening 216 defined by annular lip 218 for receiving inset 214. In this embodiment, inset 214 has a diameter less than opening 216. It will be appreciated that the connecting relationship between the port and tip can be reversed (i.e., port having annular lip for receiving tip having inset). Lip 218 defines bed 222 for
20 receiving substrate 220, which is secured in port assembly 202 when port 205 is connected to tip 215. Tip 215 includes aperture 224 in bed 222. Aperture 224 provides for contact of substrate 220 with a liquid sample contained in a sealed vessel into which port assembly is introduced. Tip 215 terminates with apex 226 that facilitates the introduction of port assembly 202 into a sealed vessel by puncture. FIGURE 4C is a plan
25 view of tip 215 illustrating bed 222 and aperture 224. In one embodiment, the assembly is made from Lexan HPS1 1125 available from GE Polymerland, Pittsfield, MA.

Representative sealed vessels incorporating the substrate-immobilized fluorescent species are illustrated in FIGURES 5A and 5B. FIGURE 5A illustrates a sealed vessel into which a port assembly has been inserted by puncture. FIGURE 5B illustrates a
30 sealed vessel manufactured to include a port assembly.

Referring to FIGURE 5A, sealed vessel 500 includes a plurality of vessel ports 510. Port assembly 202 (including port 205, membrane 220, and tip 215) resides in

vessel port 510A after insertion. Vessel 500 remains sealed after insertion of port assembly 202. Vessel port 510A seals to port 205.

Referring to FIGURE 5B, sealed vessel 500 includes a plurality of vessel ports 510. Port assembly 232 (including port 205, membrane 220, and tip 215) resides in vessel port 510A after vessel manufacture. A process for manufacturing a representative sealed vessel incorporating a port assembly is described in Example 1.

A representative port assembly useful for incorporation into a sealed vessel during manufacture is illustrated in FIGURE 6. The port assembly useful for incorporation during vessel manufacture is substantially the same as the port assembly useful for introduction into a sealed vessel illustrated in FIGURE 4, except that the assembly useful in vessel manufacture need not include, and preferably does not include, a feature for puncturing the vessel. Referring to FIGURE 6, port assembly 232 includes port 205 and tip 235. Port 205 is a cylinder terminating with window 210 and having opening 212 for receiving probe member 185 (not shown). In one embodiment, port 205 tapers from opening 212 to window 210 such that the depth of insertion of probe member 185 into port 205 is predetermined by the probe's diameter. When inserted in the port, the face of probe member 185 and window 210 are substantially parallel. Port 205 and tip 235 are adapted such that the port and tip are reversibly connectable. In one embodiment, port 205 includes annular inset 214 and tip 235 includes opening 216 defined by annular lip 218 for receiving inset 214. In this embodiment, inset 214 has a diameter less than opening 216. It will be appreciated that the connecting relationship between the port and tip can be reversed (i.e., port having annular lip for receiving tip having inset). Lip 218 defines bed 222 for receiving substrate 220, which is secured in port assembly 202 when port 205 is connected to tip 235. Tip 235 includes aperture 224 in bed 222. Aperture 224 provides for contact of substrate 220 with a liquid sample contained in the sealed vessel.

Fluorescent species having pH-dependent emission. The method and system of the invention for measuring pH uses a fluorescent species having pH-dependent fluorescent emission. The fluorescent species has a first emission intensity at a first wavelength and a second emission intensity at a second wavelength, the first and second emission intensities being characteristic of pH in the environment of the fluorescent species. The ratio of the first and second emission intensities provides pH measurement. It is appreciated that fluorescent emission occurs as a wavelength band having a band maximum that is referred to herein as the emission wavelength.

In one embodiment, the separation between the first wavelength and the second wavelength is at least about 40 nm. In one embodiment, the separation between the first wavelength and the second wavelength is at least about 30 nm. In one embodiment, the separation between the first wavelength and the second wavelength is at least about 5 20 nm. Using 10 nm HBW filters, the separation is at least about 30 nm. Preferably, the system of the invention achieve fluorescence signal separation by removing any emission band overlap by 10E5 or more.

The method and system of the invention for measuring pH are not limited to any 10 particular fluorescent species, nor any particular pH range. The method and system of the invention is operable with any fluorescent species having pH-dependent properties that can be excited and its emission measured. The range of pH measurable by the method and system of the invention can be selected and is determined by the pH-dependent properties of the fluorescent species.

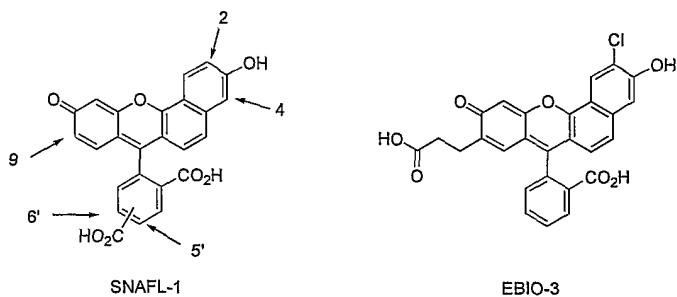
In addition to their pH-dependent properties noted above, suitable fluorescent 15 species include those that can be substantially irreversibly immobilized on a substrate. The fluorescent species can be covalently coupled to the substrate or non-covalently associated with the substrate.

Suitable pH-dependent fluorescent species include those known in the art. Representative fluorescent species having suitable pH-dependent properties include 20 fluorescein derivatives including naphthofluorescein compounds, seminaphthofluorescein compounds (e.g., SNAFL compounds), and seminaphthorhodafluor compounds (e.g., SNARF compounds). These compounds have advantages associated with their long wavelength emission, which is less susceptible to potential interfering light absorbing substances in blood. These compounds also have relatively long wavelength absorbance 25 making them particularly suitable for excitation by commercially available LED light sources. Another compound having suitable pH dependent behavior is HPTS, 8-hydroxy-1,3,6-pyrenetrisulfonic acid. Although the compound has desired ratiometric pH properties, excitation is optimal at short wavelength (403 nm) where strong LED light sources are not commercially available. Representative SNAFL and SNARF compounds 30 useful in the method and system of the invention are described in U.S. Patent No. 4,945,171. Molecular Probes (now Invitrogen, Eugene, OR) sells CNF, SNAFL, SNARF fluors with conjugatable carboxylic acid linker groups, see, for example, Molecular Probes Handbook (Ninth Edition) by R.P. Haugland, Chapter 21

"pH indicators" pages 829-847. Epoch Biosciences (now Nanogen, Bothell, WA) sells EBIO-3 with a propanoic acid linker. Whitaker et al. (Anal. Biochem. (1991) 194, 330-344) showed the synthesis of a number of SNAFL compounds. Wolfbeis et al. (Mikrochim Acta (1992) 108, 133-141) described the use of CNF and aminocellulose conjugates. The earliest reference to the SNAFL family of compounds is Whitaker et al. (1988) Biophys. J. 53, 197a. A related dye in the CNF family is VITABLUE, a sulfonenaphthofluorescein derivative (Lee et al (1989) Cytometry 10, 151-164) having a pKa of 7.56. A CNF analog with bromine substituents at each carbon adjacent to a phenol (pKa 7.45) has a pKa that is 0.54 pKa units lower than their measured pKa for CNF (pKa 7.99). Lee et al. note that "true" pKa values are difficult to determine for these compounds. A method for pKa determination is described in Example 3. SNAFL-1 (literature pKa ~ 7.8) free acid had a pKa of 7.6 in that fluorescence-based assay.

The structures of seminaphthofluorescein compounds (SNAFL-1 and EBIO-3) useful in the method and system of the invention are illustrated below.

15

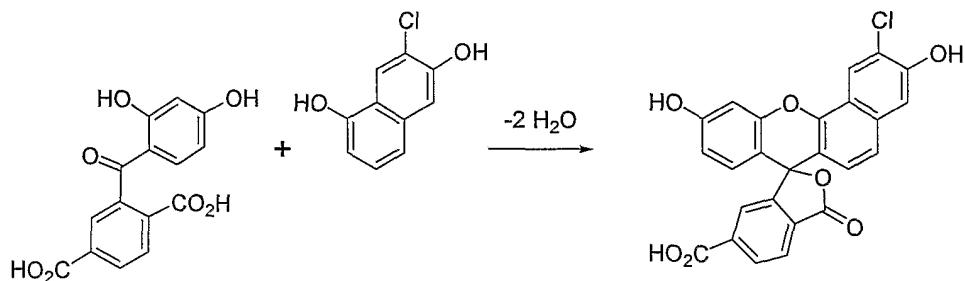


The numbering scheme describes position of attachment of linker molecules. These compounds have carboxylate linking groups suitable for conjugation to carrier proteins, as described below. For conjugation, the reactive N-hydroxysuccinimide (NHS) ester of SNAFL-1 (commercially available from Molecule Probes, Inc., Eugene, OR) can be used. Conjugation to lysine residues in human serum albumin (HSA) gave desired SNAFL/HSA conjugates. Carbodiimide activation of EBIO-3 gave a reactive intermediate that was efficiently conjugated to human serum albumin.

25 Representative naphthofluorescein and seminaphthofluorescein compounds useful
in the method and system of the invention are illustrated in FIGURE 7.

The SNAFL compounds are commercially available from Molecular Probes, Inc., Eugene, OR. The SNAFL compounds can be readily synthesized according to general procedures that have been published (see, for example, U.S. Patent No. 4,945,171).

5 The preparation of a representative 2-chloro substituted SNAFL compound is shown below.



10 The compound can be prepared by condensation of 1,6-dihydroxynaphthalene with the diacid substituted 4-acylresorcinol in the presence of a dehydrating acid or Lewis acid catalyst, such as Zinc chloride.

15 The preparation of SNAFL compounds having propionic acid linkers is described in U.S. Patent Application No. 11/022,039, incorporated herein by reference in its entirety. A representative SNAFL compounds having a propionic acid linker, EBIO-3, is commercially available from Nanogen, Bothell WA.

20 The emission spectra as a function of pH of representative fluorescent species (i.e., SNAFL-1 and EBIO-1) useful in the method and system of the invention are illustrated in FIGURES 8 and 9, respectively. FIGURE 8 illustrates the emission spectra of SNAFL-1 in 50 mM potassium phosphate buffer as a function of pH (pH 6.0 to 10.0) (excitation at 540 nm). Referring to FIGURE 8, the response at pH 6-7 is relatively poor (pKa = 7.6). FIGURE 9 illustrates the emission spectra of EBIO-3 in 50 mM potassium phosphate buffer as a function of pH (pH 6.0 to 10.0) (excitation at 545 nm). Referring to FIGURE 9, the response at pH 6-7 is relatively good (pKa = 6.6). Spectral properties and pKa data for the SNAFL analogs illustrated in FIGURES 7A-7E are summarized in 25 Table 1.

Table 1. pH-Sensitive absorbance and emission of SNAFL analogs.

Compound	Absorbance λ_{max} (acid)	Absorbance λ_{max} (base)	Emission λ_{iso}	Emission λ_{max} (base)	pKa
SNAFL-1	482, 510 nm	540 nm	585 nm	620 nm	7.6
SNAFL-2	485, 514	547	590	630	7.6
EBIO-1	496, 519	545	560	620	6.5
EBIO-2	506, 538	572	590	645	7.8
EBIO-3	480, 509	534	560	610	6.6

Referring to Table 1, absorbance and emission spectra were obtained at 10 μM 5 SNFL analog. Absorbance was measured at pH 6, 8, and 10: acid (pH 6) gave two bands of similar absorbance; pH 10 gave a single λ_{max} (base). The emission spectra were determined by excitation at the absorbance λ_{max} (base). The wavelength where emission spectra crossed is reported as λ_{iso} . The emission λ_{max} was measured at pH 10. pKa was determined from fluorescence emission spectra. EBIO-1 and EBIO-3 were more 10 sensitive to changes at pH \sim 6.5. The other analogs were more sensitive at pH \sim 8.

Fluorescent species conjugates for substrate immobilization. For use in the method and system of the invention, the fluorescent species is immobilized on a substrate such that the fluorescent species is in contact with the sample, the pH of which is to be measured. The fluorescent species can be immobilized on the substrate through the use 15 of a material (e.g., macromolecular spacer material) having a strong associative interaction with the substrate. The spacer material allows covalent conjugation of the fluorescent species and provides large surface area needed for efficient non-covalent immobilization to the substrate surface. In one embodiment, the spacer material is human serum albumin (HSA) having \sim 44 lysine residues available for covalent conjugation. 20 HSA's densely charged molecular structure has a passivating effect when adsorbed to biomaterials. Other advantages include reduced fluorescence quenching, uniform environment for the conjugated fluorophore, and availability in recombinant form (from yeast) so there is no chance of infection (as with HSA from donors). HSA conjugates are easily purified by ultrafiltration methods and form stable solutions that are easily

characterized by absorbance and fluorescence assays to determine the number of fluorophores per protein.

In one embodiment, the fluorescent species is immobilized on the substrate through the use of a protein or protein fragment. Suitable proteins include those that can be substantially irreversibly immobilized on the substrate. The protein can be covalently coupled to the substrate or non-covalently associated with the substrate. Suitable proteins include proteins to which the fluorescent species can be substantially irreversibly immobilized. The fluorescent species can be covalently or non-covalently associated with the protein.

10 Suitable proteins include human serum albumin (HSA), bovine serum albumin (BSA), von Willebrand's factor, kininogen, fibrinogen, and hemoglobin (no iron). Suitable proteins include proteins having available lysine residues (for conjugation to the fluorophore) and molecular weight sufficient to allow for immobilization efficiency to the blot membrane. Other functional groups in the protein (like cysteine) could presumably 15 be used for covalent bonding to suitably reactive solid supports.

In one embodiment, the fluorescent species is immobilized on the substrate through the use of a polysaccharide. Suitable polysaccharides include those that can be substantially irreversibly immobilized on the substrate. The polysaccharide can be covalently coupled to the substrate or non-covalently associated with the substrate. 20 Suitable polysaccharides include proteins to which the fluorescent species can be substantially irreversibly immobilized. The fluorescent species can be covalently or non-covalently associated with the polysaccharide.

Suitable polysaccharides include dextrans, aminodextrans, heparin, and lectins.

25 In another embodiment, the fluorescent species is immobilized on the substrate through the use of dendrimeric structures. Suitable dendrimeric structures include those that can be substantially irreversibly immobilized on the substrate. The dendrimeric structures can be covalently coupled to the substrate or non-covalently associated with the substrate. PAMAM dendrimers are commercially available as are other structural types and sizes.

30 In one embodiment, the fluorescent species is covalently coupled to a protein to provide a fluorophore-protein conjugate that can be immobilized on a substrate. In one embodiment, the fluorophore-polysaccharide conjugate is non-covalently associated with the substrate.

In one embodiment, a fluorophore-protein conjugate is immobilized on a substrate. In one embodiment, the fluorescent species is a seminaphthofluorescein and the protein is human serum albumin. In one embodiment, the seminaphthofluorescein is SNAFL-1. The preparation of SNAFL-1/HSA conjugates is described in Example 4.

5 The fluorescent properties of SNAFL-1/HSA conjugates are described in Example 5. In one embodiment, the seminaphthofluorescein is EBIO-3. The preparation of EBIO-3/HSA conjugates is described in Example 6. A schematic illustration of the coupling of EBIO-3 to HSA is illustrated in FIGURE 10. The fluorescent properties of EBIO-3/HSA conjugates are described in Example 7.

10 The fluorescent emission spectra as a function of pH (6.0 to 10.0) of a representative fluorophore-protein conjugate (SNAFL-1/HSA, 1.6 fluorophores per HSA) useful in the method and system of the invention are illustrated in FIGURE 11.

15 The fluorescent emission spectra as a function of pH (6.0 to 10.0) of a representative fluorophore-protein conjugate (EBIO-3/HSA, 1.92 fluorophores per HSA) useful in the method and system of the invention are illustrated in FIGURE 12.

For the fluorophore-protein conjugate, the optimum fluorophore loading will vary depending on the particular fluorophore.

20 For SNAFL-1/HSA conjugates the fluorophore loading can vary from about 0.01 to about 40 SNAFL-1/HSA. Low signal at 0.01 and fluorescent quenching at 40 fluorophores/HSA. In one embodiment, the SNAFL-1 conjugate includes about 2 SNAFL-1/HSA.

25 For EBIO-3/HSA conjugates the fluorophore loading can vary from about 0.01 to about 40 EBIO-3/HSA. In one embodiment, the EBIO-3 conjugate includes about 2 EBIO-3/HSA.

30 Substrates for fluorescent species immobilization. In the method and system of the invention, the fluorescent species is immobilized on a substrate. As noted above, the fluorescent species can be directly immobilized on the substrate covalently or by non-covalent association or, alternatively, through the use of a material (e.g., fluorophore-protein conjugate) that can be immobilized on the substrate covalently or by non-covalent association.

Suitable substrates substantially irreversible immobilized the fluorescent species. In the method of the invention, suitable substrates also do not inhibit the contact of the liquid sample with the fluorescent species and do not impair or alter the pH measurement.

Representative substrates include membranes, such as microporous membranes made of nitrocellulose, mixed esters of nitrocellulose and cellulose acetate, polyethylene terephthalate, polycarbonate, polyvinylidene fluoride and polyimide. Such materials are available commercially from Whatman S&S, Florham Park, NJ and Millipore, Billerica MA. Suitable membranes include membranes in which the microporous structure is created by ion beam penetration such as membranes commercially available from Oxyphen GmbH, Dresden, Germany under the designation OXYPHEN. Charged nylon surfaces (Nytran) can also be used. Suitable membranes include plastic membranes in which the microporous structure is made by injection molding the micropores into the plastic such as the processes used by Åmic, Stockholm, Sweden. Emission intensity of SNAFL-1/HSA at pH 7 immobilized on various pore size mixed ester nitrocellulose cellulose acetate membranes is shown in FIGURE 22.

Immobilization of representative fluorophore protein conjugates on membranes is described in Examples 8 and 10. Example 8 describes the immobilization of SNAFL-1/HSA conjugates. Example 9 describes the fluorescent properties of immobilized SNAFL-1/HSA conjugates. Example 10 describes the immobilization of EBIO-3/HSA conjugates. Example 11 describes the fluorescent properties of immobilized EBIO-3/HSA conjugates.

The emission spectra of a representative fluorophore-protein conjugate (SNAFL-1/HSA, 3.6:1) immobilized on Oxyphen and nitrocellulose as a function of pH (pH response), as measured by the microwell assay described in Example 9, are illustrated in FIGURES 13 and 14, respectively.

The emission spectra of a representative fluorophore-protein conjugate (EBIO-3/HSA, 2.0:1) immobilized on nitrocellulose, as described in Example 8, as a function of pH (6.0, 6.5, 7.0, 7.5, 8.0, and 10.0), as measured by the telescoping tube insert assay described in Example 11, are illustrated in FIGURE 15. The large spread of emissions at 600 nm for the pH 6 to 8 range indicates good fluorescence versus pH response.

Ratiometric pH Method and System. The method of the invention is a fluorescent wavelength-ratiometric method. In the method, the first and second fluorescent emission intensities of the fluorescent species measured at first and second emission wavelengths, respectively, are ratioed to provide pH information. The first emission wavelength varies with pH while the second emission wavelength is constant with pH and gives an internal

control for the fluorescent intensity. In one embodiment, a lookup table is used to lookup a combination of the measured ratio, first and second emission wavelength and determines its corresponding pH. In one embodiment, a mathematical function of the ratio, first and second emission wavelength is used to calculate the resulting pH.

5 FIGURE 16 illustrates the data used in the method of the invention for measuring pH. The emission spectra of a representative fluorophore-protein conjugate (EBIO-3/HSA, 2:1) immobilized on nitrocellulose at pH 7.0 is shown as measured by the telescoping tubing insert assay. In this setup, the excitation bandpass filter was unable to completely remove the excitation light in the emission region as illustrated by the
10 background signal measured on a blank nitrocellulose disc. The full spectrum corrected for the background was multiplied by the transmittance of the first and second hypothetical filters at each wavelength and the area under the resultant curve was calculated to give a signal for the first and second wavelength. The center wavelengths and bandwidths of hypothetical filters were chosen such that the ratiometric properties of
15 the conjugate had the strongest relationship to the pH in the region of interest.

FIGURE 17 illustrates the results of the method of the invention for phosphate buffered saline (PBS), platelet poor plasma (PPP), and platelet rich plasma (PRP) as measured by the telescoping tubing insert assay described in Example 11. The three curves represent the best fit relationship between the measured pH and ratios for the three
20 different liquids.

FIGURE 18 illustrates the correlation of pH results for three different plasma samples obtained by the method and system of the invention as measured by the injection molded insert PVC tube assay described in Example 11. The relationship between the fluorescent signal and the pH has an accuracy of about 0.1 pH units.

25 FIGURE 19 illustrates stability of a representative substrate-immobilized fluorophore conjugate of the invention (EBIO-3/HSA, 2:1) on mixed ester nitrocellulose and cellulose acetate prepared by the soaking method and as measured by the leaching assay described in Example 10. The low level of leaching is far below the toxic level for any compound.

30 Carbon dioxide measurement. In another aspect, the present invention provides a device and method for measuring carbon dioxide concentration in a liquid sample. The carbon dioxide measuring method utilizes the pH measuring method and system described above. In the carbon dioxide measuring method and device, a

substrate-immobilized fluorescent species as described above is in contact with a solution, the pH of which is responsive to carbon dioxide level. In addition to being in contact with the substrate-immobilized fluorescent species, the solution having pH responsive to carbon dioxide level is in contact with a liquid sample for which the 5 level of carbon dioxide is to be measured. The solution having pH responsive to carbon dioxide level is isolated from the liquid sample for which the level of carbon dioxide is to be measured by a selectively permeable membrane. The membrane is permeable to gases (e.g., carbon dioxide) and impermeable to other materials (e.g., liquids). Using the method of measuring pH described above, the pH of the solution responsive to carbon 10 dioxide concentration in contact with the substrate-immobilized fluorescent species is measured and correlated with the carbon dioxide level of the sample in contact with that solution.

The solution having pH response to carbon dioxide level is an aqueous solution that includes an agent that is reactive toward carbon dioxide and changes the pH of the 15 solution in response to carbon dioxide concentration. Suitable agents that are reactive toward carbon dioxide and change the pH of the solution in which they are dissolved include bicarbonates, such as sodium bicarbonate.

The selectively permeable membrane isolates the solution having pH responsive to carbon dioxide level from the liquid sample containing carbon dioxide. The membrane 20 is permeable to carbon dioxide and impermeable to liquids and other solutes. In the method, carbon dioxide from the liquid sample passes from the liquid sample through the membrane and into the aqueous solution thereby reacting with the carbon dioxide reactive agent to alter the pH of the aqueous solution. Suitable selectively permeable membranes include membranes made from silicone and PTFE.

25 FIGURE 20 illustrates a representative device of the invention for measuring carbon dioxide in a sealed vessel. Referring to FIGURE 20, device 600 includes port assembly 610 including port 620 and tip 630. Port 620 is a cylinder terminating with window 622 and having opening 624 for receiving probe member 185. When inserted in the port, the face of probe member 185 and window 622 are substantially parallel. 30 Port 620 and tip 630 are adapted such that the port and tip are reversibly connectable. Substrate 640 including immobilized fluorescent species is secured within port 620 and tip 630. Tip 630 includes a chamber 645 for receiving a solution having pH responsiveness to carbon dioxide. Chamber 645 is defined by window 622, tip 630, and

selectively permeable membrane 650. Chamber 645 includes substrate 640, which is interrogated by probe member 185.

A device for measuring carbon dioxide was assembled as described above with the membrane containing immobilized EBIO-3/rHSA conjugate (rHSA is recombinant HSA). A layer of PARAFILM M, a blend of olefin-type materials, was added under the membrane towards the tip. The membrane was hydrated with 5 ul of 35 mM carbonate buffer (pH 7.4), which was sealed within the assembly by the PARAFILM M and remained hydrated throughout the assay. The assembly was subjected to 100% carbon dioxide gas by connection to the gas source with tubing and a "Y" adapter to bleed off the pressure. The assembly was subjected to the carbon dioxide for an allotted period of time, allowed to acclimate to ambient air conditions, and repeated. The fluorescence was measured at each stage at 568 nm and 600 nm after being excited at 525 nm. The results are summarized below in Table 2 and reflect changes in fluorescence due to the change in carbon dioxide concentration demonstrating that the fluorometric ratio method of the invention can also be used to calculate carbon dioxide concentration. The PVC storage bags that are used for platelet storage are somewhat gas permeable, and carbon dioxide is directly related to the measurement of pH.

Table 2. Carbon dioxide sensing results.

Environmental Conditions	EM at 568 nm	EM at 600 nm	Ratio (600/568)
15 min. at Ambient CO ₂	753	2184	2.9
5 min. at 100% CO ₂	1179	2234	1.894
15 min. at Ambient CO ₂	833	2175	2.611
8 min. at 100% CO ₂	1161	1930	1.662
60 min. at Ambient CO ₂	765	2184	2.854

20

The present invention provides a fluorescence-based pH indicator that can be easily inserted into the sampling ports of designed blood storage bags and interrogated using a fiber optic-based LED light source and photodiode measurement system. This solid state system uses a "ratiometric" calibration method that accounts for variability in 25 fluorescent signal strength due to interfering substances in blood that may interfere with the amount of excitation light that hits the indicator dye. The ratio of fluorescence

intensities are measured at two wavelengths, one to detect the acid (protonated) isomer of the dye and one to detect the base (deprotonated) isomer.

To develop an accurate pH detector for platelet rich plasma, compounds having pKa of ~ 6.6 are suitable, for example, 2-chloro substitution of SNAFL compound lowers the pKa of the phenol from 7.6 to ~ 6.6. Conjugates of these compounds can be immobilized to various solid supports to provide sensing pH membranes.

The present invention provides an inexpensive, easy to manufacture pH sensing membrane that gives accurate measurement of pH in platelet storage bags at pH 6.5-7.5. In one embodiment, the invention uses a protein conjugate (human serum albumin) of a 10 2-chloro substituted ratiometric fluorescent compound. The fluorophore:HSA ratio was optimized for performance when immobilized to a nitrocellulose blot membrane. After drying on the membrane, the fluorophore:HSA conjugate has very low leaching rates. Discs of this material are easily assembled into holders for insertion into the sampling 15 ports of platelet storage bags. The fluorescent membrane materials showed good pH response using a green LED based fluorometer. In the method, two emission wavelengths for ratiometric pH detection are measured with properly filtered photodiodes with an accuracy of ~0.1 units at the desired low pH threshold of 6.5.

Fluorescent probe molecules can be designed to be sensitive to a variety of environments. The method and system of the invention describes the use of pH-sensitive 20 fluorophores. However, other environments can be interrogated by the method and system of the invention modified to include environment-sensitive fluorophores other than pH-sensitive fluorophores. A variety of fluorescent probes that change fluorescent properties as the molecular environment changes are commercially available. See, for example, Molecular Probes Handbook (9th Edition) by R.P. Haugland. Probes can be 25 linked to albumins or other proteins and used to prepare substrates for interrogation as described in herein or using other fluorescent-based methods. Examples of environment-sensitive fluorophores, systems, and methods include the following.

Nucleic acid detection: nucleic acid binding dyes change fluorescent properties in the presence of DNA or RNA.

30 Enzyme substrates: proteins or peptides can be labeled with fluorescent dyes and fluorescent quenching molecules such that a fluorescent signal is generated in the presence of particular enzymes such as proteases (FRET detection).

Probes for lipids: lipophilic dyes can change fluorescent properties in the presence of cell membranes or other lipid rich analytes.

5 Probes for oxygen: in addition to pH detection and carbon dioxide detection, certain fluorescent molecules are sensitive to changes in oxygen concentration, for example, tris(2,2'-bipyridiyl)ruthenium(II) dichloride (RTDP).

Indicators for metal ions: fluorescent dyes that bind metals can change fluorescent properties upon binding calcium, magnesium, zinc, sodium, potassium, among other.

10 Glucose detection: certain lectins such as ConA bind glucose, and suitably labeled lectins can be prepared as probes for glucose.

The following examples are provided for the purposes of illustrating, not limiting, the invention.

EXAMPLES

Example 1

15 The Manufacture of a Vessel Incorporating a Representative Substrate-Immobilized Fluorescent Species

Referring to FIGURE 5B, sealed vessel 500 is manufactured from PVC. PVC material is compounded with a number of additives, for example, plasticizers, stabilizers, and lubricants. The formulation is used for making bags and tubes. The compounded 20 PVC is extruded through a die for converting the plasticized material into sheet form. The extruded sheet, after slitting, is cut into the desired size and sent to the welding section. The donor and transfer tubings are made by extrusion of similar PVC compounds. The tubes are then cut to the appropriate length and sent to the welding section. The components, such as transfusion ports, needle covers, and clamp, are 25 produced by injection molding. The components are ultrasonically cleaned and dried in a drying oven.

Welding. The blood bags are fabricated by a high frequency welding technique. Sized PVC sheets are placed between electrodes and high frequency at high voltage is applied. PVC gets heated very rapidly and sealing takes place between electrodes. 30 Transfusion ports and donor and transfer tubing are kept in the appropriate position with the bag and welded to form an integral part of the blood bag system. For the manufacture of a vessel incorporating a representative substrate-immobilized fluorescent species (FIGURE 5B), an open tube is welded to provide port 510A. The tube can be made of

colored PVC to provide light protection for the immobilized fluorescent species. Welded bags are trimmed. The port assembly 232 (FIGURE 6) is manufactured from injection molded Lexan parts (205 and 235) and a 3.53 mm (9/64 inch) diameter nitrocellulose disc with immobilized fluorescent species (220). The port assembly is held together by 5 friction fit or can be glued in place. The port assembly is inserted in the open tube of port 510A. The port assembly is held in the port by friction fit or can be glued in place. The assembled bag and port assembly is sterilized and labeled for ultimate storage of platelet concentrates.

Example 2

10 The Incorporation of a Representative Substrate-Immobilized
Fluorescent Species into a Sealed Vessel

Referring to FIGURE 5A, sealed vessel 500 includes a plurality of vessel ports 510. Port assembly 202 resides in vessel port 510A after insertion. The port assembly 202 (FIGURES 4A-4C) is manufactured from injection molded Lexan parts (205 and 15 215) and a 3.53 mm (9/64 inch) diameter nitrocellulose disc with immobilized fluorescent species (220). The port assembly is held together by friction fit or can be glued in place. The port assembly is inserted through the septum seal inside port 510A by puncturing the seal with the spiked tip. Alternatively, the seal can be pre-punctured with a separate spike tool. The insertion of the port assembly can be performed on either empty or 20 platelet filled bags, but in either case, aseptic methods should be used to avoid possible contamination of the bag contents. The port assembly is held in the port by friction fit or can be glued in place. Vessel 500 remains sealed (leakproof) after insertion of port assembly 202 in port 510A.

Example 3

25 Fluorescence and pH Properties of Representative SNAFL Analogs:
pKa determination

Instrumentation. Fluorescence versus pH of various SNAFL free acids were compared using an Ocean Optics USB2000 fiber optic spectrometer and a tungsten halogen light source (part number HL-2000 FHS). The light source was equipped with 30 a linear variable filter that allowed the wavelength and shape of the excitation beam to be adjusted. The excitation wavelength was adjusted by using a blank cuvette to the absorbance max of the fluorophore (see Table 1). A cuvette holder (part number CUV-FL-DA) was directly attached to the light source and a fiber optic cable directed

emitted light to the spectrometer. Excitation conditions are reported for each fluorescence spectrum (3000 msec irradiation at the indicated wavelength). Spectral data were collected on a personal computer using the Ocean Optics software and overlays of different spectra were captured.

5 Sample preparation. SNAFL-1 was purchased as the free carboxylic acid from Molecular Probes in a 1 mg vial. 0.3 mL of isopropyl alcohol and 0.7 mL of water was added to make a 1 mg/mL solution. A molecular weight (MW) of 426 for SNAFL-1 was used to calculate molarity (SNAFL-1 = 2.35 mM). 4.25 uL of this solution was diluted to 1 mL with various 50 mM phosphate buffers to give 10 micromolar solutions with
10 pH 6-10. 10 micromolar solutions of SNAFL-2 (MW= 460) were prepared in a similar fashion. EBIO-1 (MW=523), EBIO-2 (MW=627), and EBIO-3 (MW=489) were obtained as bulk compounds from Epoch Biosciences. 1.6 mg of each solid powder was carefully weighed out and dissolved in 3.2 mL of 40% isopropyl alcohol to give 0.5 mg/mL solutions. Emission spectra were obtained for the various SNAFL and
15 EBIO compounds at pH 6.0, 6.2, 6.4, 6.6, 6.8, 7.0, 8.0 and 10.0. Examples of overlayed fluorescence emission spectra are shown in FIGURE 8 (SNAFL-1) and FIGURE 9 (EBIO-3). All spectra showed an isosbestic wavelength where all emission spectra overlap (See Table 1). This is a characteristic of ideal ratiometric performance with no competing fluorescent structures other than those shown above (lactone, naphthol,
20 naphtholate).

25 pKa calculations. The pH at which two molecular species (tautomers) are equally represented is defined as the pKa. There are many variables that can affect pKa and methods for measurement are difficult since the structures have overlapping absorbance. Therefore direct comparisons from the literature can vary slightly. The calculations contained herein are based on the assumption that, at pH 10, only the trianionic naphtholate structure is present. The intensity of fluorescence at the emission maxima is divided by 2, and pH of the intersecting pH curve is calculated by interpolation between the nearest 2 curves. The pKa of the 2-chloro substituted EBIO compounds is significantly lower than the other analogs as shown in Table 1.

Example 4The Preparation of Representative Fluorophore-Protein Conjugates: SNAFL-1/HSA

Human serum albumin (HSA) was purchased from Sigma (catalog # A-8763) as 100 mg of lyophilized powder. SNAFL-1 NHS ester was purchased from Molecular Probes as a mixture of the 5 and 6 isomers. A solution of 10 mg (0.15 micromoles) of HSA in 1 mL of pH 8.56 sodium bicarbonate (0.1 M) was prepared. A solution of 1 mL (1.91 micromoles) of the NHS ester in 0.1 mL of dimethylsulfoxide was prepared. 0.3 mL aliquots of the HSA solution were transferred to a 1.6 mL Eppendorf tubes and various offering ratios of the NHS ester solution were added: tube 1, 11.8 microliters (5 equivalents); tube 2, 23.6 microliters (10 equivalents), tube 3, 47.1 microliters (20 equivalents). The deep red solutions were vortexed and allowed to stand in the dark for at least one hour. The 5:1 conjugate from tube 1 was purified by gel filtration chromatography on a 0.5 x 20 cm column packed with Sephadex G-15 and pH 7.4 phosphate buffered saline (PBS). The conjugate was isolated as a fast moving red / orange band in PBS and diluted to 0.75 mL with PBS to give a 4 mg/mL solution of the protein conjugate. Most of the color eluted with the conjugate, but some small molecular weight (orange) impurities remained on top of the column. The column was clean enough to be re-used for purification of the 10:1 and 20:1 conjugates. Each was eluted in PBS and diluted to 0.75 mL to give ~4 mg/mL solutions (60 micromolar based on HSA component). The red solutions were stored refrigerated and protected from light. 1 micromolar solutions of each SNAFL-1 / HSA conjugate were prepared and analyzed by UV-vis spectra using a Beckman DU640B spectrometer. Each spectrum showed absorbance maxima at 490 and 521 nm at pH 7 as expected for the acid form of SNAFL-1 conjugates. The relative absorbance showed the expected change in absorbance with different SNAFL:HSA offering ratio. A 10 micromolar solution of SNAFL-1 acid (obtained from Molecular Probes) at pH 7 was used as a standard to more accurately determine the average loading of SNAFL-1 per each HSA conjugate preparation. Using this assay, the 5:1 conjugate had 4.1 fluors/HSA, the 10:1 conjugate had 6.4 fluors/HSA, and the 20:1 conjugate had 11.2 fluors /HSA.

Example 5The Fluorescent Properties of Representative Fluorophore-Protein Conjugates:
SNAFL-1/HSA

Relative fluorescence of various SNAFL-1/HSA conjugates and SNAFL-1 free acid were compared using an Ocean Optics USB2000 fiber optic spectrometer and a tungsten halogen light source (part number HL-2000 FHS). The light source was equipped with a linear variable filter that allowed the wavelength and shape of the excitation beam to be adjusted. A cuvette holder (part number CUV-FL-DA) was directly attached to the light source and a fiber optic cable directed emitted light to the spectrometer. Excitation conditions are reported for each fluorescence spectrum (3000 msec irradiation at the indicated wavelength). Spectral data were collected on a personal computer using the Ocean Optics software and overlays of different spectra were captured. A comparison of various loading levels of SNAFL-1/HSA showed that 4.1 to 1.6 SNAFL-1 molecules gave about the same fluorescent signal. Higher loading or lower loading conjugates gave lower signals.

Emission spectra were obtained for 10 micromolar solutions in potassium phosphate buffer. Excitation was at 540 nm. Emission maximum at 620 nm was observed for the base form of SNAFL-1 (pH 10). As expected, intensity of 620 nm fluorescence decreased as pH decreased. An isosbestic point at 585 nm, where fluorescence remained constant at all pH, was observed. Response was good at about pH 8, but poor between pH 6-7.

Spectra obtained for a 2.5 micromolar solution of a representative SNAFL-1/HSA conjugate (1.6 SNAFL-1/HSA) showed improved pH response for pH 6-7 (see FIGURE 11). The Ocean Optics halogen light source was equipped with a 532 nm interference filter (Edmund Optics, Barrington, NJ.) and this allowed the fluorescent isosbestic point at 572 nm for pH 6-7 to be detected. Emission maximum at 620 nm was observed for the base form of SNAFL-1 (see pH 10 curve). As expected, intensity of 620 nm fluorescence decreased as pH decreased. In comparison to the free SNAFL-1 carboxylic acid (see FIGURE 8) improved response for pH 6-7 was observed for the HSA conjugate. A red shift of the pH 8 and 10 curves from the isosbestic wavelength was observed, indicative of other competing molecular structures involving the fluorescent species. This non-ideal behavior may be eliminated by use of a longer linker structure or a more hydrophilic linker structure between the fluorescent dye and the HSA spacer.

Example 6The Preparation of Representative Fluorophore-Protein Conjugates: EBIO-3/HSA

Method A. A 0.1 M stock solution of EDC (Sigma/Aldrich Chemical Co., St. Louis MO) was prepared by dissolving 6.2 mg of EDC in 0.2 mL of DMF and 0.123 mL of 50 mM phosphate buffer (pH 5.8). 1.0 mg of EBIO-3 acid (Nanogen, Bothell, WA) was dissolved in 0.102 mL of DMF to give a 20 mM solution. 3.0 mg (0.045 micromoles) of HSA (Sigma/Aldrich Chemical Co., St. Louis, MO) was dissolved in 0.3 mL of pH 8.5 sodium bicarbonate in each of two 1.7 mL Eppendorf tubes. 0.1M EDC (0.045 mL) was added to 20 mM EBIO-3 (0.045 mL, 0.9 micromoles) in a 10 separate Eppendorf tube and this was added to one of the HSA tubes to give an EBIO-3:HSA offering ratio of 20:1. An offering ratio of 5:1 was used in the other HSA tube by adding a premixed solution of 0.0225 mL of EDC (0.1 mM) and 0.0225 mL of 15 EBIO-3 (20 mM). The homogeneous dark red HSA conjugate solutions were incubated at room temperature in the dark. After 21 hours, each of the HSA conjugates was purified on a G15 Sephadex column as described above for the SNAFL conjugates (Example 4). Some unreacted EBIO-3 acid remained at the top of the column (especially for the 20:1 offering ratio), but was cleanly separated from the desired protein conjugate that eluted first as a pink fraction in ~0.5 mL of pH 7.4 buffer. Each of the purified conjugates was diluted to 0.75 mL with pH 7.4 PBS to give 4 mg/mL solutions 20 (0.06 mM). The red solutions were stored refrigerated and protected from light. 1 micromolar solutions of each EBIO-3 / HSA conjugate were prepared at pH 7.4 and analyzed by UV-vis spectra using a Beckman DU640B spectrometer. The free EBIO-3 acid (10 micromolar) spectrum had absorbance maximum at 534 nm, the 20:1 conjugate had absorbance at 538 nm and the 5:1 conjugate had maximum at 545 nm. The spectra 25 showed the expected increase in absorbance with increasing EBIO-3:HSA offering ratio. Using this EBIO-3 acid as a standard, the 20:1 conjugate had 5.07 EBIO-3:HSA and the 5:1 offering had 1.92 EBIO-3:HSA. The coupling efficiency was somewhat lower than for the SNAFL/HSA conjugates of Example 4 (the 20:1 conjugate had 11.2 fluors/HSA and the 5:1 offering had 4.1 fluors/HAS). The EDC coupling method was suitably 30 efficient and reproducible.

Method B. A 0.1 M solution of EDC (Sigma/Aldrich Chemical Co., St. Louis, MO) is prepared by dissolving 6.0 mg of EDC in 0.194 mL of DMF and 0.118 mL of 50 mM PBS (pH 7.4). 3.0 mg of EBIO-3 acid (Nanogen, Bothell, WA) is dissolved in 0.306

mL of DMF to give a 20 mM solution. The two solutions are combined in the EBIO-3 solution container and incubated at room temperature for one hour in the dark. 75.0 mg (1 micromole) of liquid recombinant HSA (rHSA) from yeast (Delta Biotechnology, Ltd., Nottingham, UK) is mixed with 7.5 mL of pH 8.5 sodium bicarbonate in a 15 mL conical tube. The entire contents of the EBIO-3/EDC solution are combined with the rHSA solution and incubated at room temperature in the dark for 15-20 hours. The rHSA/EBIO-3 conjugate is purified using the Amicon stirred ultrafiltration cell system and a YM10 membrane (Millipore, Bedford, MA). A 50 mM PBS (pH 7.4) is used as the wash solution. After purification, the protein concentration of the conjugate is measured 10 using the BCA™ Protein Assay (Pierce, Rockford, IL). An aliquot of the conjugate is diluted to 1 mg/ml with 50 mM PBS (pH 7.4) based on its BCA determined protein concentration. The 1 mg/ml aliquot of conjugate, the last milliliter of PBS effluent, an aliquot of the 50 mM PBS (pH 7.4), and an aliquot of the EB3 Standard (15 mM EBIO-3 solution in DMF and 50 mM PBS (pH 7.4)) are analyzed via an absorbance scan utilizing 15 Bio-Tek's Synergy HT plate reader. The scan is taken on 300 microliters of each of the above mentioned samples in a black, 96-well, clear, flat bottom plate, scanned from 450 nm to 650 nm. Their max peaks are recorded and used to determine purity and quality of the conjugate.

Example 7

20 The Fluorescent Properties of Representative Fluorophore-Protein Conjugates:

EBIO-3/HSA

Fluorescence spectra were obtained for 2.5 micromolar solutions of the two EBIO-3/HSA conjugates prepared as described in Example 6 (Method A). The conjugates showed improved pH response for pH 6-7 (see FIGURE 12 for overlayed 25 spectra for the 1.92:1 EBIO-3/HSA conjugate). The Ocean Optics halogen light source was equipped with a 532 nm bandpass filter (Edmund Optics, Barrington NJ.) and this allowed the fluorescent isosbestic point at ~565 nm for pH 6-7 to be detected. Emission maximum at 605 nm was observed for the base form of SNAFL-1 (red trace, pH 10). As expected, intensity of 605 nm fluorescence decreased as pH decreased. In comparison to 30 the SNAFL-1/HSA conjugate (see FIGURE 11) improved response for pH 6-7 was observed for the EBIO-3/HSA conjugate. A red shift of the pH 8 and 10 curves from the isosbestic wavelength was observed, indicative of other competing molecular structures

involving the fluorescent species, but was of smaller magnitude than for the SNAFL-1/HSA conjugate.

Example 8

Immobilization of Representative Fluorophore-Protein Conjugates: SNAFL-1/HSA

5 Fluorophore-protein conjugates and fluorophore-carbohydrate conjugates were immobilized on either nitrocellulose or capillary pore membranes using the following general method. Fluorescein labeled dextrans with "fixable" lysine residues were obtained from Molecular Probes. These dextrans had a molecular weight of about 10,000 1.8 fluorophores per conjugate, and 2.2 lysines per conjugate and are sold under the trade 10 name "Fluoro-Emerald". Fluorescein labeled bovine serum albumin (BSA) was also obtained from Molecular Probes and had 4.5 fluors per conjugate. Various SNAFL-1/HSA conjugates were prepared as described in Example 4. Nitrocellulose membranes were obtained from Schleicher and Schuell under the trade name PROTRAN. Pore diameter was reported as 0.2 microns. Capillary pore membranes made from 15 polyester films were obtained from Oxyphen in a variety of pore sizes. 0.1 micron and 1.0 micron pore size membranes were successfully used to immobilize fluorescein dextrans. Fluorescein/dextran, fluorescein/BSA and SNAFL-1/HSA conjugates were all successfully immobilized and the fluorescent properties of the SNAFL-1/HSA conjugates were fully characterized as described as follows.

20 General Immobilization Method. SNAFL-1/HSA (2.5 SNAFL-1/HSA) on 0.1 micron pore diameter Oxyphen Membrane Discs. Fluorescent HSA conjugates with a 2.5:1 SNAFL-1:HSA offering ratio were prepared as described in Example 4 and diluted to provide concentrations of 0.05, 0.2, 1.0 and 4 mg/mL in phosphate buffered saline (PBS) (pH 7.4). 5 microliter drops were applied via a 20 microliter pipettor to the center 25 of pre-punched porous discs (1/4 inch diameter) that were laid on a bench top. The spotted discs were allowed to air dry (about 30 minutes) and then placed in separate desiccators overnight. The dried discs were washed in separate Eppendorf tubes with 2x1 mL of PBS and allowed to soak overnight in 1 mL of PBS. The washed discs were stable in PBS solution (no degradation after 30 days). Alternatively the discs could be re- 30 dried in desiccators and stored dry. The wet or dry stored discs had comparable fluorescent properties. The discs had fluorescent signals that were proportional to the concentration of labeled macromolecule applied to each one as measured by the fluorescence assay described in Example 9.

Example 9The Fluorescent Properties of Representative Immobilized Fluorophore-Protein Conjugates:
SNAFL-1/HSA

5 Microwell assay of fluorescent macromolecular conjugates on porous membrane discs using a fiber optic spectrometer. Fluorescent discs prepared as described in Example 8 were examined for fluorescent properties using the Ocean Optics fiber optic spectrometer described in Example 5. The cuvette on the light source was replaced by a fiber optic reflectance probe which had 6 excitation fibers wrapped around a single fiber
10 that picks up the emitted light from the sample and sends it to the spectrometer. The reflectance probe was threaded through a hole in a 12x12x18 inch black box with a lid on the front. The probe was clamped inside under a 1 cm square opening that allowed the tip of the probe to be positioned under a 96-well micro well plate (clear bottom black plate). The probe was tilted at a 30 degree angle to reduce reflected light entering the probe tip.
15 The fluorescent disc of interest was placed in the bottom of a well and covered with 300 microliters of the analyte solution of interest. The excitation light source was turned on long enough to position the disc of interest over the tip of the reflectance probe, then the shutter was closed and the plate was covered with another box to shield the disc from ambient light. Unless otherwise mentioned, the Ocean Optics software was set to collect
20 data with a 3000 msec integration time and 3 averages. A dark spectrum was captured with the shutter closed and used for all background subtracted readings during the assay. The shutter was then opened and fluorescent reading of the disc was started. The graphical display on the computer screen gave real-time spectra after each 3000 msec integration time. After the required 3 spectra were obtained (about 10 seconds) the
25 graphical display showed only subtle changes. At this point a snapshot of the displayed spectrum was captured and saved to disc for future processing. The shutter was closed, and the next microwell experiment was set up. The same disc could be measured multiple times by exchanging the analyte solution in the microwells. Alternatively, different discs in different wells could be measured by re-positioning the microwell plate
30 over the reflectance probe.

Fluorescent loading of SNAFL-1/HSA immobilized on Oxyphen discs. The microwell assay described above was used to compare the relative-fluorescence of SNAFL-1/HSA on Oxyphen discs. The excitation filters in the halogen light source were

set to a wavelength of 532 nm and a "wide open" bandpass position to maximize sensitivity of the assay. Reflectance of the excitation beam back into the detector fiber was significant, and the wavelength position of the filter was adjusted to provide a "minimum" at 620 nm where the fluorescence from the base form of SNAFL-1/HSA is 5 greatest. The various concentrations of SNAFL-1/HSA described in Example 8 were examined in separate microwells in pH 7 potassium phosphate buffer (50 mM) as described above. The spectra showed the ability to distinguish relative fluorescence intensity of 4, 1, 0.2 and 0.05 mg/mL membranes at pH 7. All had signal greater than background.

10 Relative fluorescence intensity of various amounts of SNAFL-1/HSA (2.5:1) immobilized on porous Oxyphen discs at pH 7. The fluorescent intensity was measured at 620 nm, the fluorescent maximum of the base form of the fluorophore. Excitation used a wide open setting on the halogen lamp that efficiently excites both acid and base forms of SNAFL-1. The reflected light from the source (unmodified disc) had the lowest 15 intensity spectrum. The spectrum of the 0.05 mg/mL disc gave a small increase in fluorescence intensity. The 0.2 mg/mL disc, 1 mg/mL disc, and 4 mg/mL disc showed stepwise increases in fluorescence intensity. The fluorescence spectra of two 30 day PBS soaked sample (1 mg/mL) from a different batch of membranes were essentially the same and showed that membrane loading was reproducible from batch to batch, and that the 20 SNAFL-1/HSA conjugates did not dissociate significantly from the disc surface in PBS solution.

25 pH Dependent fluorescence of SNAFL-1 / HSA immobilized on Oxyphen discs. The 1 mg/mL SNAFL-1/HSA discs described above were examined for pH dependent response in the microwell assay. A single disc was examined in potassium phosphate buffers of pH 4, 5, 6, 7, 8, 9, and 10. The data showed that these membrane discs had a wide dynamic range of pH measurement, but had more sensitive response at pH > 6. The time between buffer exchanges was 5 min, and there was no significant change in spectra after additional equilibration time. This showed that the response time for even dramatic changes in the pH environment of the immobilized SNAFL-1 / HSA conjugates is rapid.

30 "Crossover assay" for fluorescence measurement of pH using SNAFL-1/HSA Oxyphen discs. The microwell assay described above was used to examine the fluorescent isosbestic properties of the discs. For this assay, the shutter assembly in Ocean Optics halogen light source (part number HL-2000 FHS) was removed, and two

532 nm bandpass filters (Edmund Scientific) were inserted in the cavity using a special adaptor. This dramatically reduced the reflected background in the spectral region of interest (> 550 nm). The data shown are for 4 mg/mL loading discs prepared with SNAFL:HSA (5:1) conjugate. The immobilized protein conjugate showed unusual pH 5 vs. fluorescence properties in comparison to the solution phase data. Instead of a fluorescent isosbestic point at 575 nm, there was a stepwise increase in the fluorescent intensity as pH increased. The pH 10 spectrum showed the expected maximum at 620 nm, and crossed the overlaid spectral curves obtained in pH 4, 6, 7 and 8 buffers. These "crossover points" were used as the basis for a sensitive assay to determine pH of 10 the membrane environment. Three different membrane discs were examined using this assay format on three different days. The crossover points were reproducible within 2 nm.

15 The 4 mg/mL discs (3.6:1 SNAFL-1:HSA) showed stepwise increase in pH 10 "crossover". The crossover was at 579 nm for pH 4. Three discs/three different days gave the same result \pm 2 nm. The crossover points were at 592 nm (pH 6), 600 nm (pH 7a,b), and 611 nm (pH 8). The fluorescent maximum at pH 10 was at 620 nm, similar to the solution phase properties.

Example 10

Immobilization of Representative Fluorophore-Protein Conjugates: EBIO-3/HSA

20 Spotting Immobilization Method. EBIO-3/HSA conjugate was prepared as described in Example 6 at a ratio of 2:1. Nitrocellulose membranes were obtained from Schleicher and Schuell under the trade name PROTRAN. The discs were treated in the same way as the general immobilization method described in Example 5 using a 4 mg/ml solution of EBIO-3/HSA.

25 Soaking Immobilization Method. EBIO-3/HSA conjugate was prepared as described in Example 6 at a ratio of 2:1. Mixed ester nitrocellulose and cellulose acetate membranes were obtained from Millipore under the product series TF. The EBIO-3/HSA conjugate is diluted to 0.2 mg/ml and 45 ml is added to a 9 cm disc of the membrane. The disc is agitated overnight at room temperature and protected from light. The 30 unbound conjugate is removed and the disc is washed with two 1 hour washes and one overnight wash all with agitation. The disc is then desiccated and stored dry. Smaller discs are punched from the 9 cm disc for studies.

Example 11The Fluorescent Properties of Representative Immobilized Fluorophore-ProteinConjugates:EBIO-3/HSA

5 Telescoping tubing insert assay of fluorescent macromolecular conjugates on porous membrane discs using a fiber optic spectrometer. Fluorescent discs prepared as described in Example 10 were examined to relate the fluorescent properties to the liquid phase pH using the Ocean Optics fiber optic spectrometer described in Example 9 with the dual 532 nm filtered (Edmund Scientific) halogen light source (part number HL-2000
10 FHSA). A holder for a 5/32 inch membrane disc was crafted with 4 mm OD and 5 mm OD polystyrene telescoping tubing and an angled 0.015 in thick polystyrene window. The angled window was placed so that it held the membrane disc at a 60 degree angle relative to the tubing axis. This allows the fiber optic probe to be placed in one end of the tubing and interrogate the disc on the other side of the window which is contact with a
15 liquid of a certain pH. Buffers of known pH values were placed in contact with the telescoping tubing inserts and discs made by the spotting immobilization method in Example 10 and fluorescent emissions recorded with the Ocean Optics software set to collect data with a 1000 msec integration time and 3 averages.

For liquids with unknown pH values, a stirred and light protected vessel
20 containing 5 telescoping tubing inserts and discs made by the soaking immobilization method in Example 10, 50 mL of buffer or plasma, and a calibrated pH electrode (ROSS electrode/Orion 720a meter) was used to study the pH and fluorescent response of the fluorescent discs. Drops of 1 N HCl or 1 M NaOH were added to create a range of pHs from liquids studied. Fluorescent spectra were collected through Ocean Optics macros in
25 Excel set to read for 1000 msec integration time and three averages. The spectra were analyzed using the modeled bandpass filters and ratiometric method in Excel to obtain calibration curves for PBS, platelet poor plasma and platelet rich plasma.

Injection molded insert PVC tube assay of fluorescent macromolecular conjugates on porous membrane discs using a custom optimized fluorescence based pH detector.

30 Injection molded polycarbonate parts were fashioned to fix the fluorescent discs to the fluorescence pH detector probe as pictured in FIGURE 4. Membranes were prepared as described in the soaking immobilization method in Example 10 and assembled into the plastic insert. A 1 in long and 3/16 in ID PVC tube was placed on the spike end of the

insert such that 250 ul of liquid was placed in the tube and covered with parafilm to slow carbon dioxide desorption. A fluorescent measurement of the first and second wavelengths was taken and then the pH was read by a blood gas analyzer (Bayer 348). The pH of plasma samples were adjusted by acid and base additions as in the telescoping 5 tubing insert assay to create the range of pH data.

While the preferred embodiment of the invention has been illustrated and described, it will be appreciated that various changes can be made therein without departing from the spirit and scope of the invention.

The embodiments of the invention in which an exclusive property or privilege is claimed are defined as follows:

1. A method for measuring the pH of a sample, comprising:

(a) irradiating a fluorescent species immobilized on a substrate with excitation light emanating from a probe physically isolated from the fluorescent species immobilized on the substrate,

wherein the fluorescent species immobilized on the substrate is in liquid communication with a sample,

wherein the excitation light has a wavelength sufficient to effect fluorescent emission from the fluorescent species,

wherein the fluorescent species exhibits a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength, the ratio of the first and second emission intensities being dependent on pH; and

(b) measuring the first and second emission intensities to determine the pH of the sample.

2. The method of Claim 1, wherein the probe is physically isolated from the fluorescent species immobilized on the substrate by a window transparent to the excitation light and the fluorescent emission.

3. The method of Claim 1, wherein the probe comprises one or more optical fibers.

4. The method of Claim 1, wherein the fluorescent species is selected from the group consisting of a naphthofluorescein compound and a seminaphthorhodamine compound.

5. The method of Claim 1, wherein the naphthofluorescein compound is selected from the group consisting of a seminaphthofluorescein compound and a carboxynaphthofluorescein compound.

6. The method of Claim 1, wherein the fluorescent species is a seminaphthofluorescein compound selected from the group consisting of 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one

and 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthen-7-yl)benzoic acid.

7. The method of Claim 1, wherein the fluorescent species immobilized on a substrate comprises a conjugate of a fluorescent species and a macromolecule.

8. The method of Claim 7, wherein the macromolecule is an albumin.

9. The method of Claim 1, wherein the fluorescent species immobilized on a substrate comprises a seminaphthofluorescein/human serum albumin conjugate.

10. The method of Claim 1, wherein the sample comprises blood or a blood product.

11. The method of Claim 1, wherein the sample is contained within a sealed vessel.

12. A system for measuring pH, comprising:

(a) a light source for exciting a fluorescent species, wherein the fluorescent species has a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength;

(b) a first emission detector for measuring the first emission intensity;

(c) a second emission detector for measuring the second emission intensity;

(d) an excitation lightguide for transmitting excitation light from the light source to the fluorescent species, wherein the lightguide comprises a first terminus proximate to the light source and a second terminus distal to the light source;

(e) a first emission lightguide for transmitting emission from the fluorescent species to the first emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;

(f) a second emission lightguide for transmitting emission from the fluorescent species to the second emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;

(g) a probe housing the distal termini of the excitation lightguide, first emission lightguide, and second emission light guide; and

(h) an assembly for receiving the probe, the assembly comprising:

(i) a housing for receiving the probe, wherein the housing is adapted for receiving the probe at a first end and terminating with a window at the second end, the window being transparent to the excitation and the emission light,

(ii) a tip member reversibly connectable to the housing's second end, wherein the tip member is adapted to receive liquid from a sample to be measured, and

(iii) a fluorescent species immobilized on a substrate intermediate the tip member and the window, wherein the fluorescent species immobilized on the substrate is in liquid communication with the sample during the measurement, and wherein the window physically isolates the probe member from the fluorescent species immobilized on the substrate.

13. The system of Claim 12, wherein the light source is a light-emitting diode.
14. The system of Claim 12, wherein the first and second detectors are photodiodes.
15. The system of Claim 12, wherein the excitation lightguide, the first emission lightguide, and the second emission lightguide are optical fibers.
16. The system of Claim 12, wherein the housing comprises a tapered tube terminating with the window.
17. The system of Claim 12, wherein the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.
18. The system of Claim 12, wherein the tip member comprises a spike for puncturing a sealed vessel.
19. An assembly, comprising
 - (a) a housing having a first open end and a second closed end, wherein the closed end comprises a window transparent to visible light;
 - (b) a tip member reversibly connectable to the housing closed end, wherein the tip member is adapted to expose the housing window; and

(c) a fluorescent species immobilized on a substrate intermediate the housing window and tip member.

20. The assembly of Claim 19, wherein the housing is tapered.

21. The assembly of Claim 19, wherein the tip member comprises a spike for puncturing a sealed vessel.

22. The assembly of Claim 19, wherein the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

23. A blood bag or blood product bag, comprising the assembly of any one of Claims 19-22.

24. A conjugate, comprising an environment-sensitive fluorophore covalently coupled to an albumin.

25. The conjugate of Claim 24, wherein the environment-sensitive fluorophore is selected from the group consisting of a pH-sensitive fluorophore, an oxygen-sensitive fluorophore, a nucleic acid-sensitive fluorophore, an ion-sensitive fluorophore, a glucose-sensitive fluorophore, a lipid-sensitive fluorophore, and an enzyme-sensitive fluorophore.

26. The conjugate of Claim 24, wherein the environment-sensitive fluorophore is selected from the group consisting of a naphthofluorescein compound and a seminaphthorhodamine compound.

27. The conjugate of Claim 24, wherein the environment-sensitive fluorophore is selected from the group consisting of a seminaphthofluorescein compound and a carboxynaphthofluorescein compound.

28. The conjugate of Claim 24, wherein the environment sensitive-fluorophore is selected from the group consisting of 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one and 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthen-7-yl)benzoic acid.

29. The conjugate of Claim 24, wherein the albumin is a serum albumin.

30. The conjugate of Claim 24, wherein the albumin is a human serum albumin.
31. The conjugate of Claim 24, wherein the albumin is a recombinant human serum albumin.
32. The conjugate of Claim 24, wherein the environment-sensitive fluorophore is 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthene-7-yl)benzoic acid and the albumin is human serum albumin.
33. A membrane-immobilized fluorescent species, comprising a conjugate of a naphthofluorescein compound and an albumin adhered to a membrane.
34. The membrane-immobilized fluorescent species of Claim 33, wherein the membrane is a microporous membrane.
35. The membrane-immobilized fluorescent species of Claim 33, wherein the membrane is selected from the group consisting of nitrocellulose, mixed esters of nitrocellulose and cellulose acetate, polyethylene terephthalate, polycarbonate, and polyimide.
36. The membrane-immobilized fluorescent species of Claim 33, wherein the naphthofluorescein compound is selected from the group consisting of a seminaphthofluorescein compound and a carboxynaphthofluorescein compound.
37. The membrane-immobilized fluorescent species of Claim 33, wherein the naphthofluorescein compound is selected from the group consisting of 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one and 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthene-7-yl)benzoic acid.
38. The membrane-immobilized fluorescent species of Claim 33, wherein the albumin is a serum albumin.
39. The membrane-immobilized fluorescent species of Claim 33, wherein the albumin is a human serum albumin.

40. The membrane-immobilized fluorescent species of Claim 33, wherein the albumin is a recombinant human serum albumin.

41. A method for measuring the carbon dioxide level in a liquid sample, comprising:

(a) irradiating a fluorescent species immobilized on a substrate with excitation light emanating from a probe physically isolated from the fluorescent species immobilized on the substrate,

wherein the fluorescent species immobilized on the substrate is in liquid communication with a solution having pH responsiveness to carbon dioxide present in a liquid sample,

wherein the solution having pH responsiveness to carbon dioxide is in communication with the liquid sample through a selectively permeable membrane,

wherein the excitation light has a wavelength sufficient to effect fluorescent emission from the fluorescent species,

wherein the fluorescent species exhibits a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength, the ratio of the first and second emission intensities being dependent on pH;

(b) measuring the first and second emission intensities to determine the pH of the solution having pH responsiveness; and

(c) correlating the pH of the solution having pH responsiveness to the carbon dioxide level in the sample.

42. The method of Claim 41, wherein the probe is physically isolated from the fluorescent species immobilized on the substrate by a window transparent to the excitation light and the fluorescent emission.

43. The method of Claim 41, wherein the probe comprises one or more optical fibers.

44. The method of Claim 41, wherein the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

45. The method of Claim 41, wherein the seminaphthofluorescein is selected from the group consisting of 5'(and 6')-carboxy-3,10-dihydroxy-spiro[7H-

benzo[c]xanthene-7,1'(3'H)-isobenzofuran]-3'-one and 2-(2-chloro-3-hydroxy-9-carboxyethyl-10-oxo-10H-benzo[c]xanthen-7-yl)benzoic acid.

46. The method of Claim 41, wherein the sample comprises blood or a blood product.

47. The method of Claim 41, wherein the sample is contained within a sealed vessel.

48. A system for measuring carbon dioxide level in a liquid sample, comprising:

- (a) a light source for exciting a fluorescent species, wherein the fluorescent species has a first emission intensity at a first emission wavelength and a second emission intensity at a second emission wavelength;
- (b) a first emission detector for measuring the first emission intensity;
- (c) a second emission detector for measuring the second emission intensity;
- (d) an excitation lightguide for transmitting excitation light from the light source to the fluorescent species, wherein the lightguide comprises a first terminus proximate to the light source and a second terminus distal to the light source;
- (e) a first emission lightguide for transmitting emission from the fluorescent species to the first emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;
- (f) a second emission lightguide for transmitting emission from the fluorescent species to the second emission detector, wherein the lightguide comprises a first terminus proximate to the detector and a second terminus distal to the detector;
- (g) a probe housing the distal termini of the excitation lightguide, first emission lightguide, and second emission light guide; and
- (h) an assembly for receiving the probe, the assembly comprising:
 - (i) a housing for receiving the probe, wherein the housing is adapted for receiving the probe at a first end and terminating with a window at the second end, the window being transparent to the excitation and the emission light,

(ii) a tip member reversibly connectable to the housing's second end, wherein the tip member comprises a chamber for receiving a solution having pH responsiveness to carbon dioxide present in a liquid sample,

wherein the solution having pH responsiveness to carbon dioxide is in liquid communication with the liquid sample through a selectively permeable membrane, and

(iii) a fluorescent species immobilized on a substrate intermediate the tip member and the window,

wherein the fluorescent species immobilized on the substrate is in liquid communication with the solution having pH responsiveness to carbon dioxide during the measurement, and

wherein the window physically isolates the probe member from the fluorescent species immobilized on the substrate.

49. The system of Claim 48, wherein the light source is a light-emitting diode.

50. The system of Claim 48, wherein the first and second detectors are photodiodes.

51. The system of Claim 48, wherein the excitation lightguide, the first emission lightguide, and the second emission lightguide are optical fibers.

52. The system of Claim 48, wherein the housing comprises a tapered tube terminating with the window.

53. The system of Claim 48, wherein the selectively permeable membrane is permeable to carbon dioxide.

54. The system of Claim 48, wherein the fluorescent species comprises a seminaphthofluorescein/human serum albumin conjugate.

55. The system of Claim 48, wherein the tip member comprises a spike for puncturing a sealed vessel.

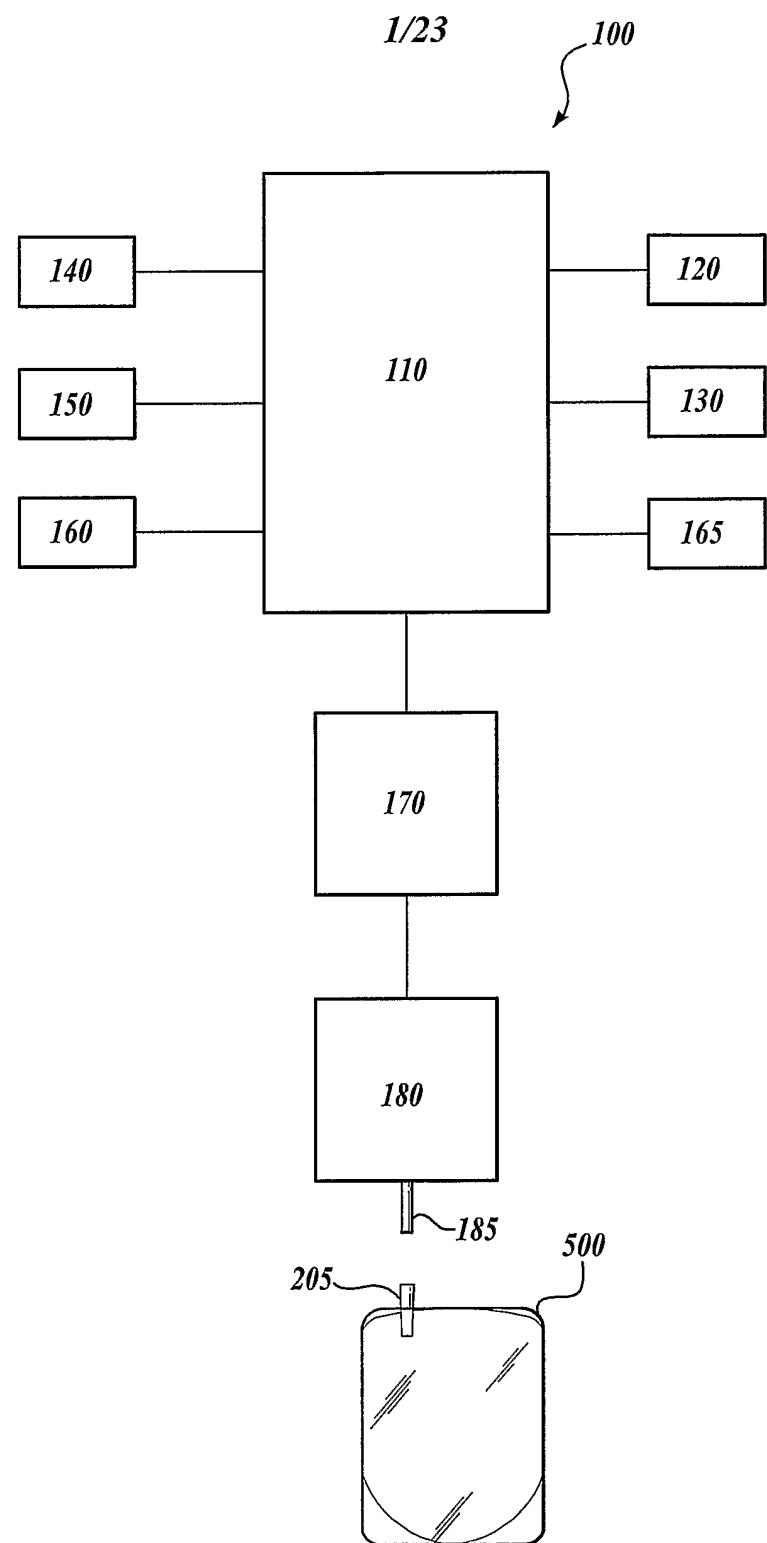
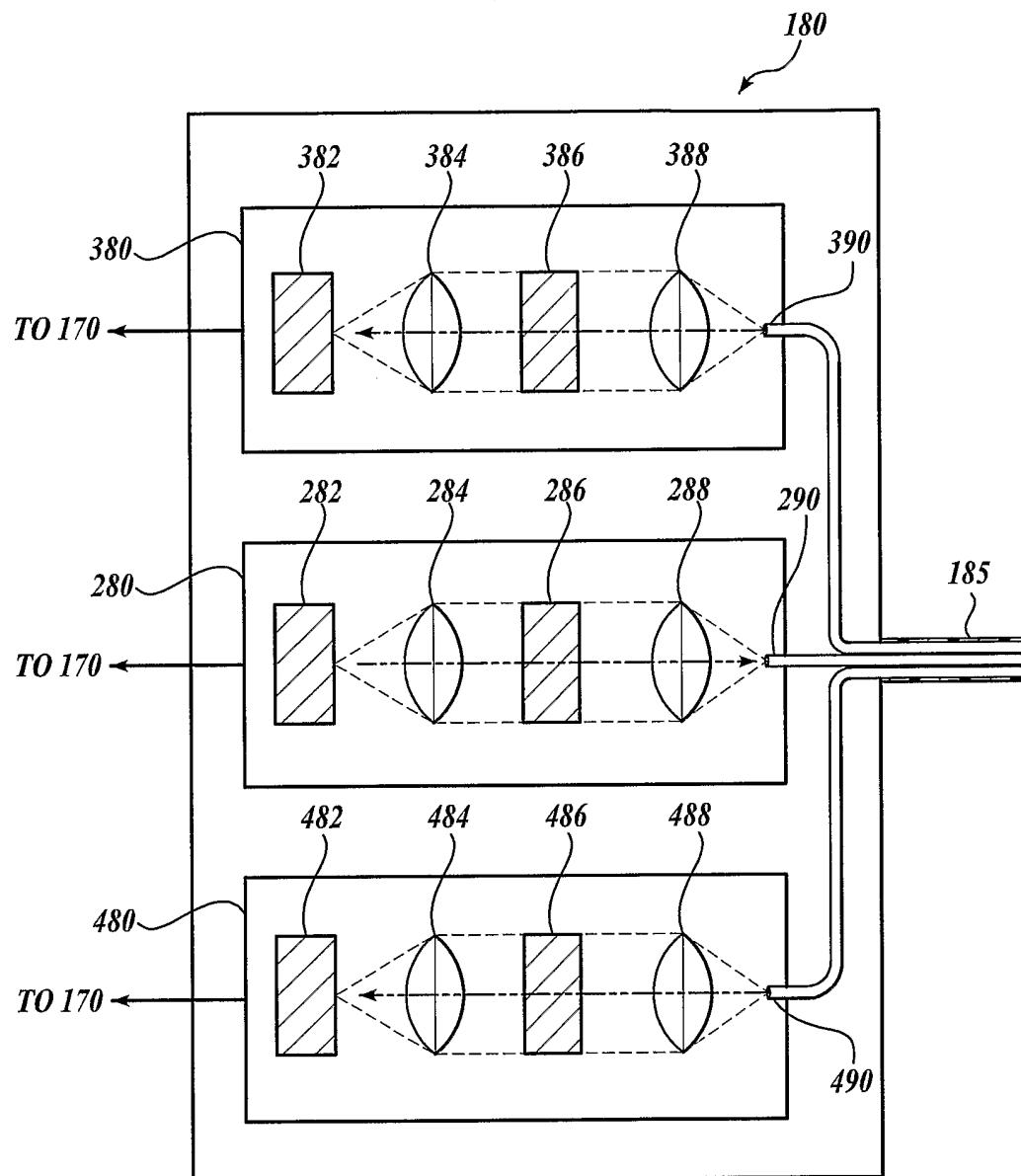
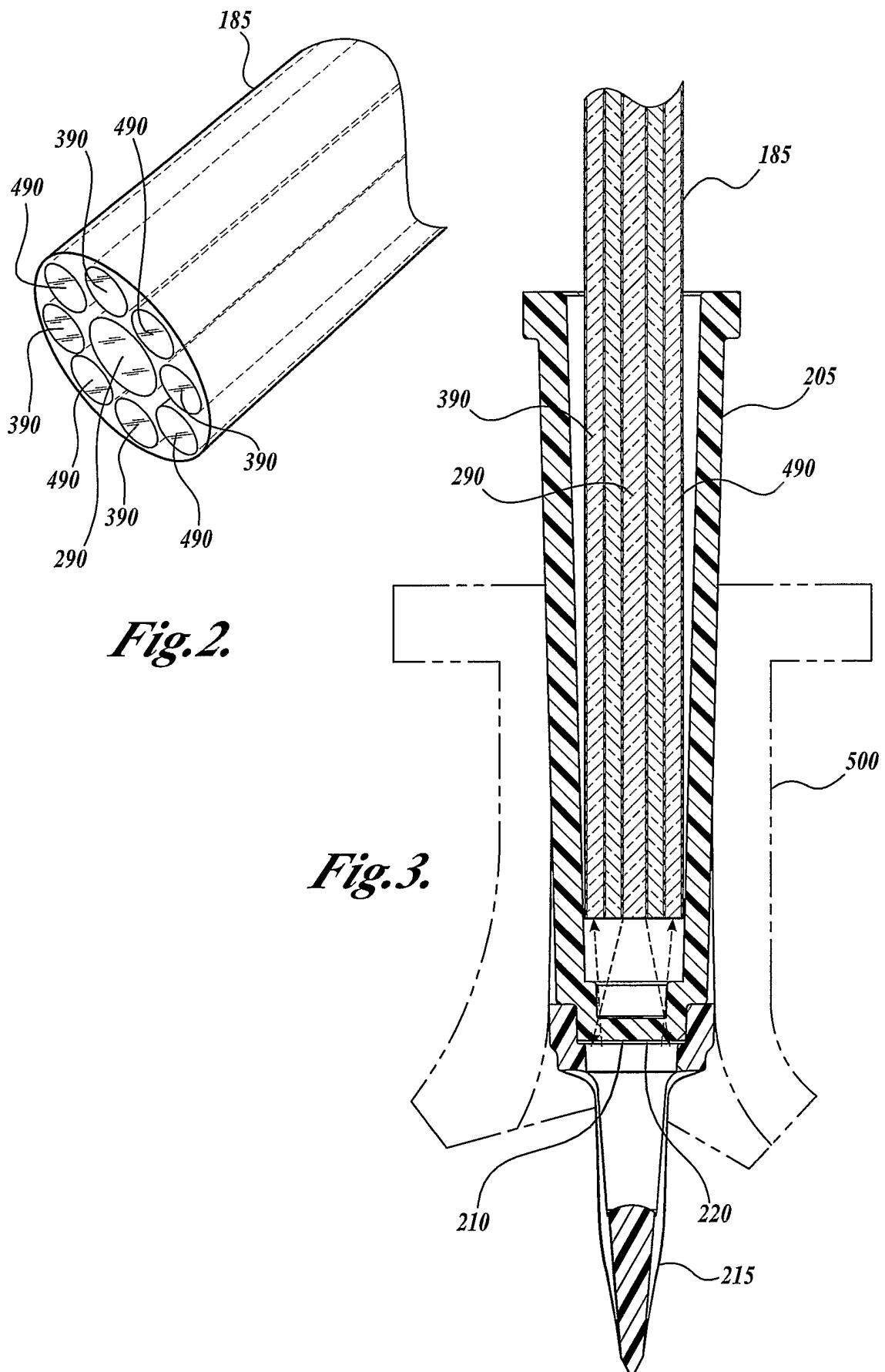


Fig. 1A.

2/23

*Fig. 1B.*

3/23



4/23

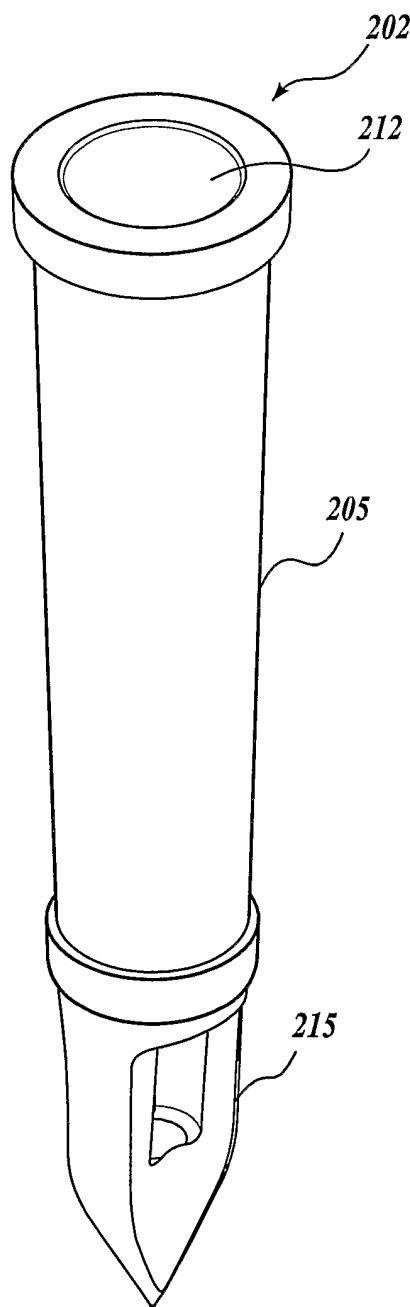


Fig. 4A.

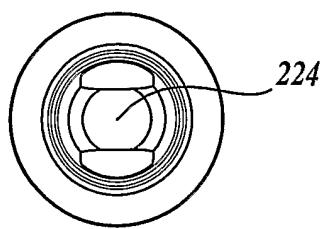


Fig. 4C.

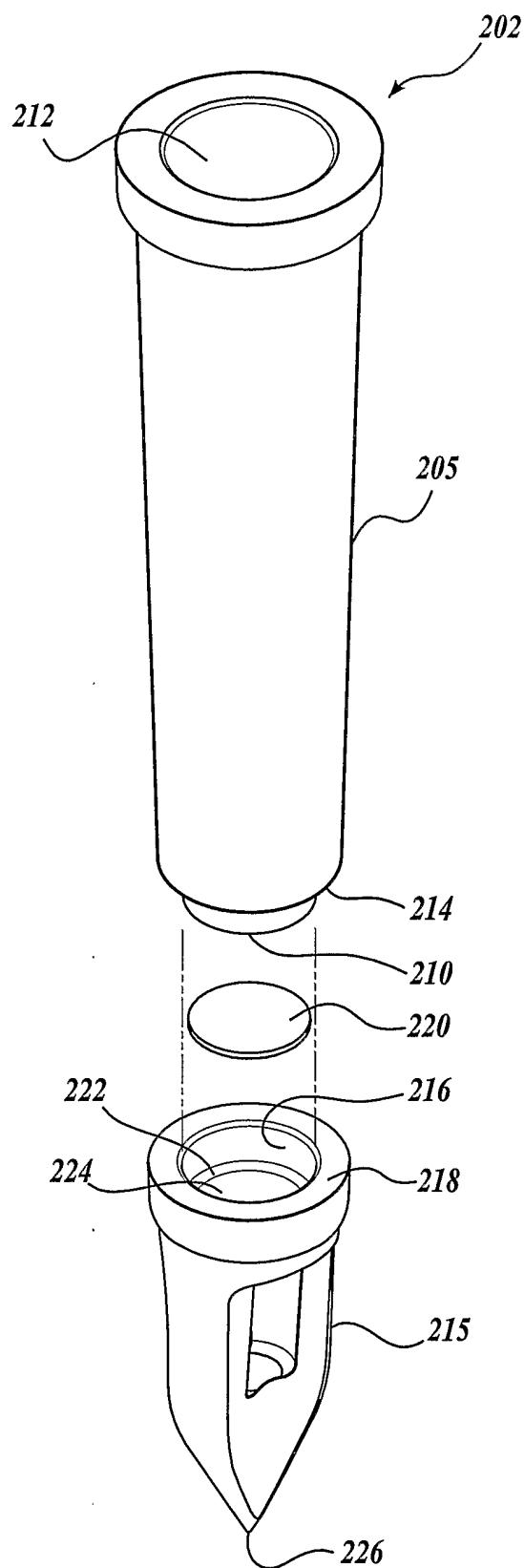


Fig. 4B.

5/23

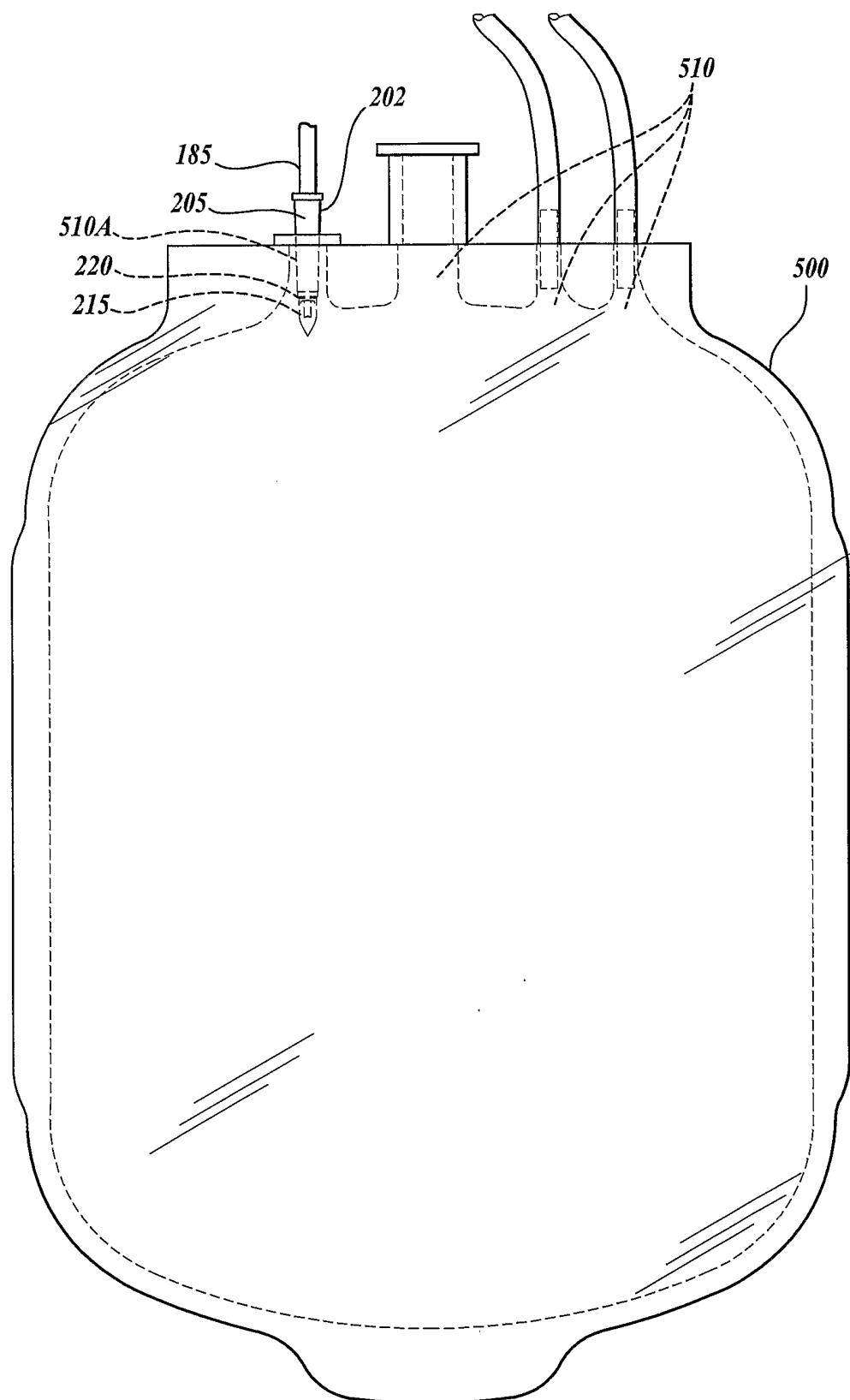


Fig. 5A.

6/23

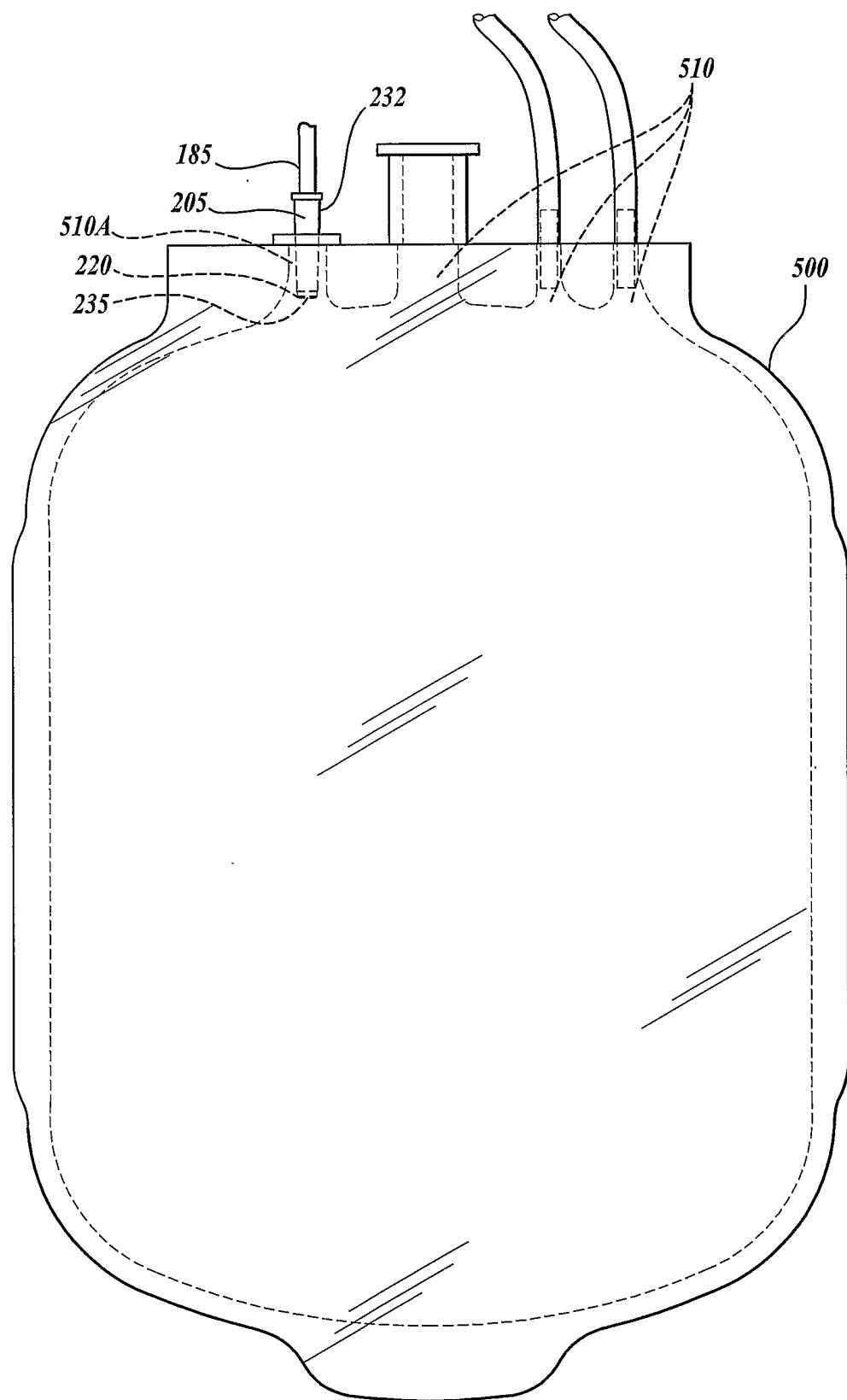


Fig. 5B.

7/23

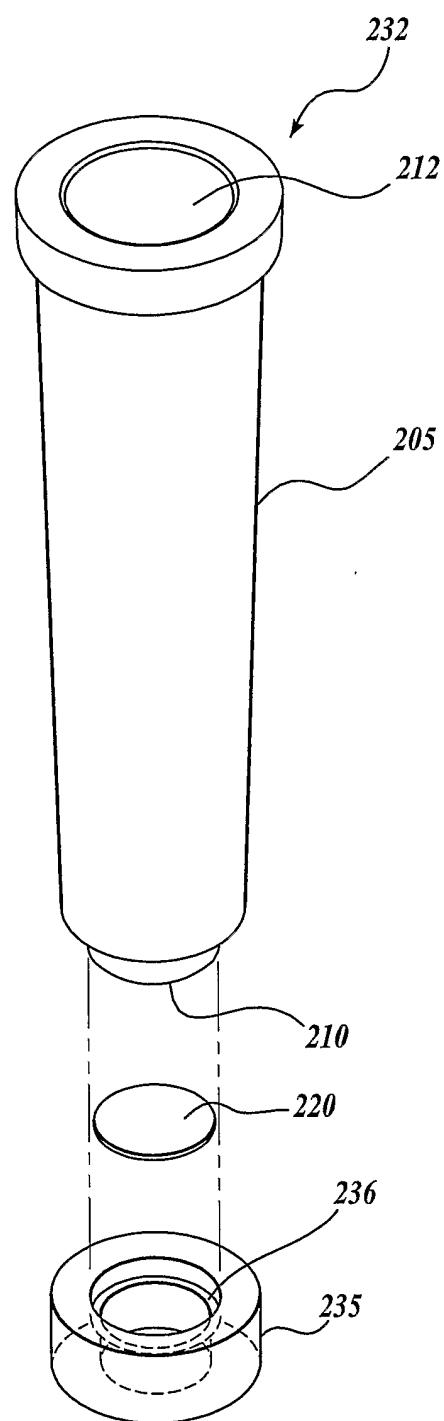


Fig. 6.

8/23

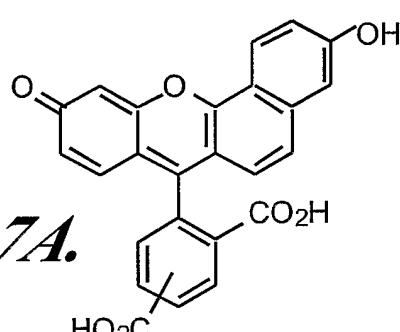


Fig. 7A. SNAFL-1

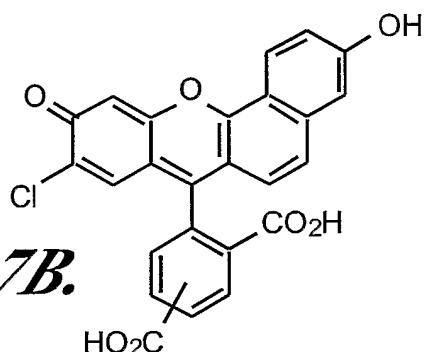


Fig. 7B. SNAFL-2

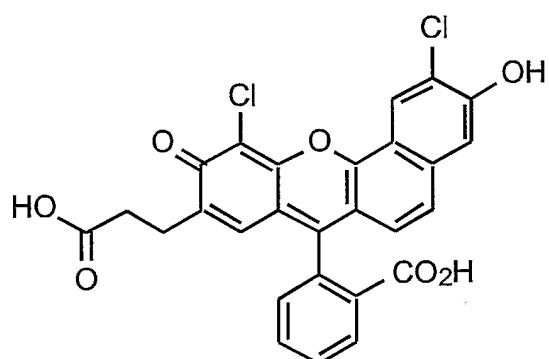


Fig. 7C. EBIO-1

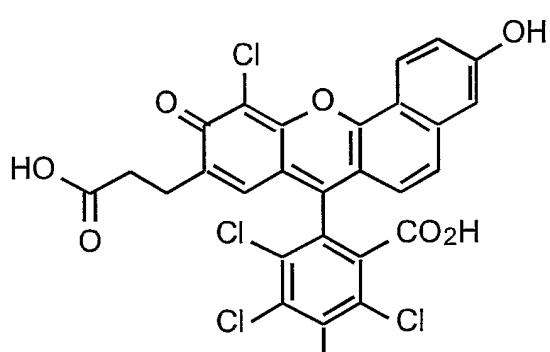


Fig. 7D. EBIO-2

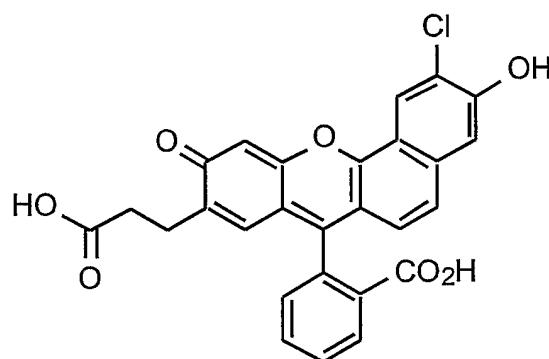


Fig. 7E. EBIO-3

9/23

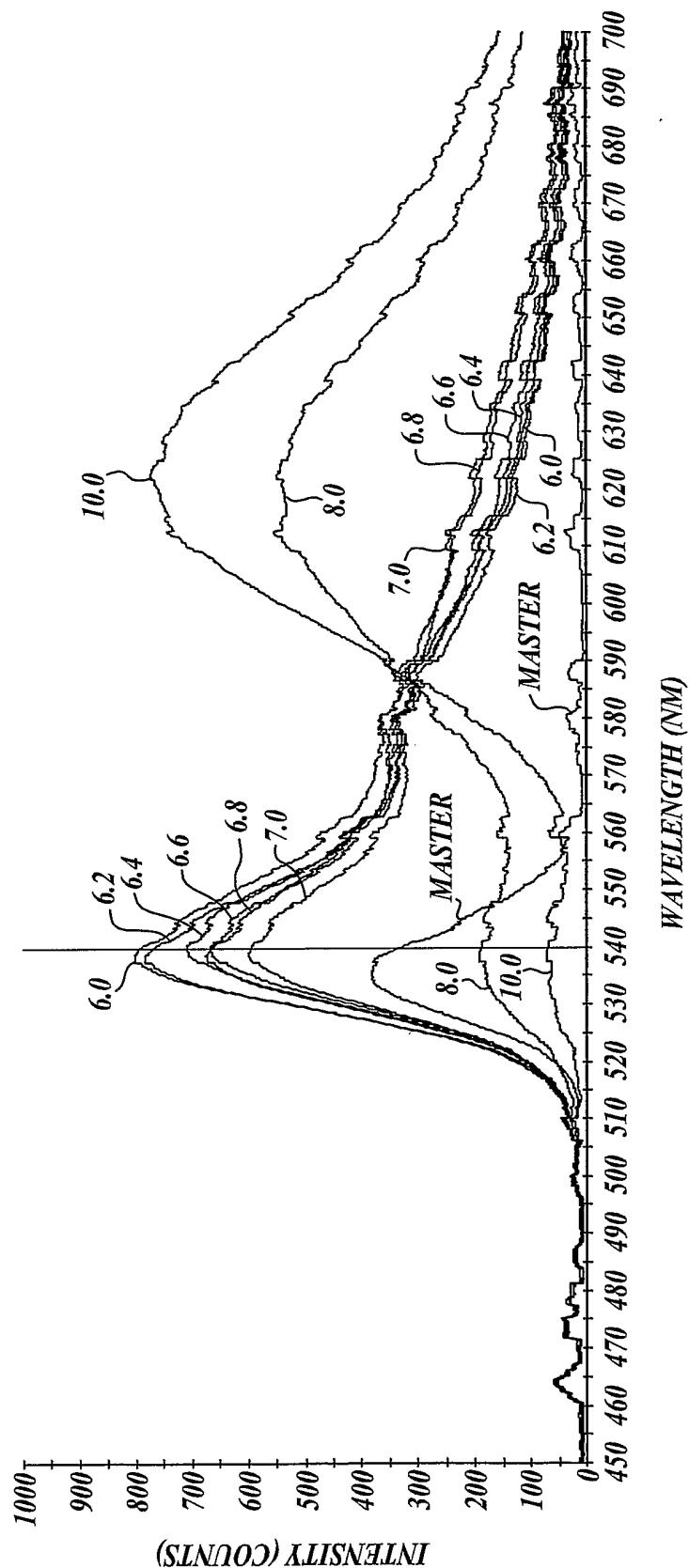


Fig. 8.

10/23

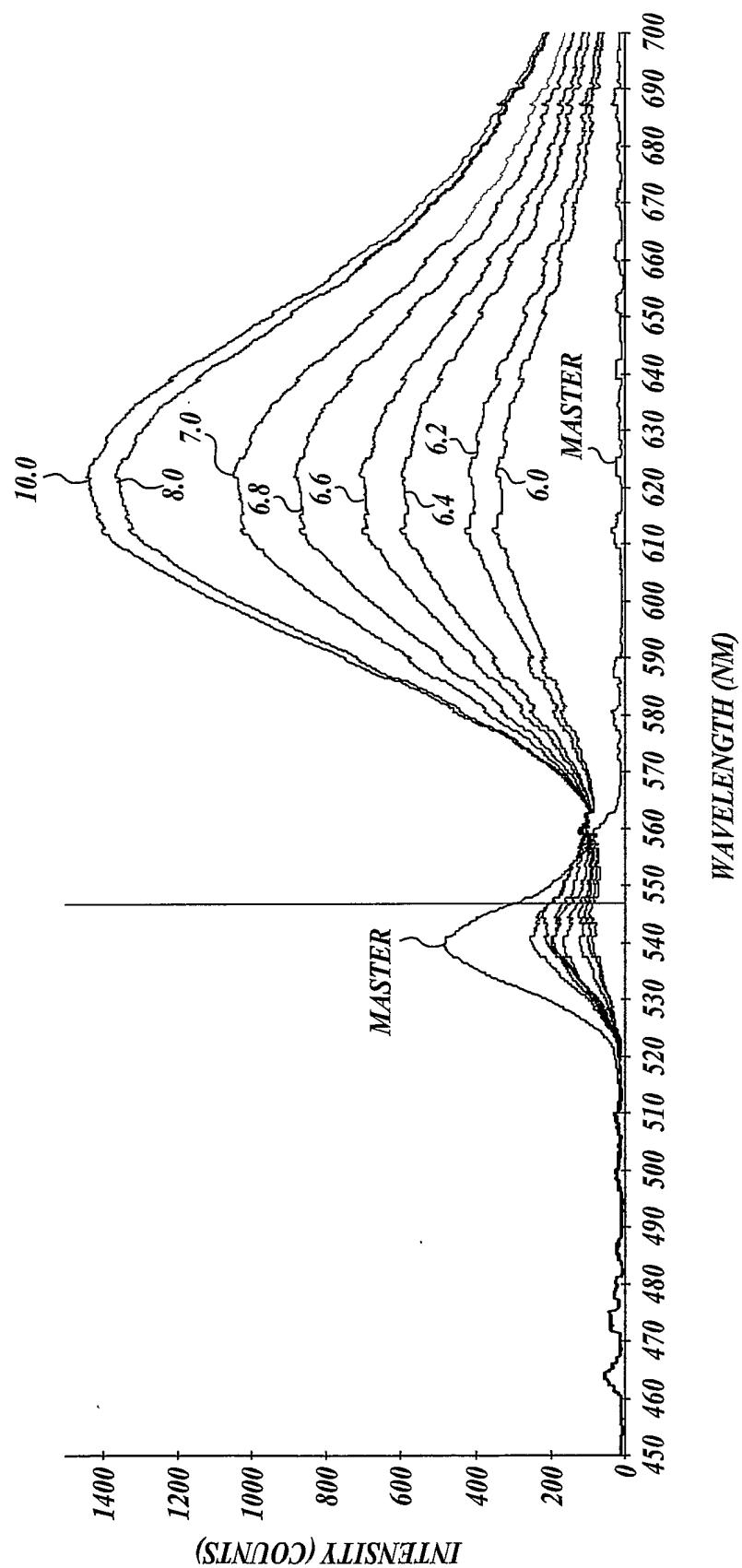


Fig. 9.

11/23

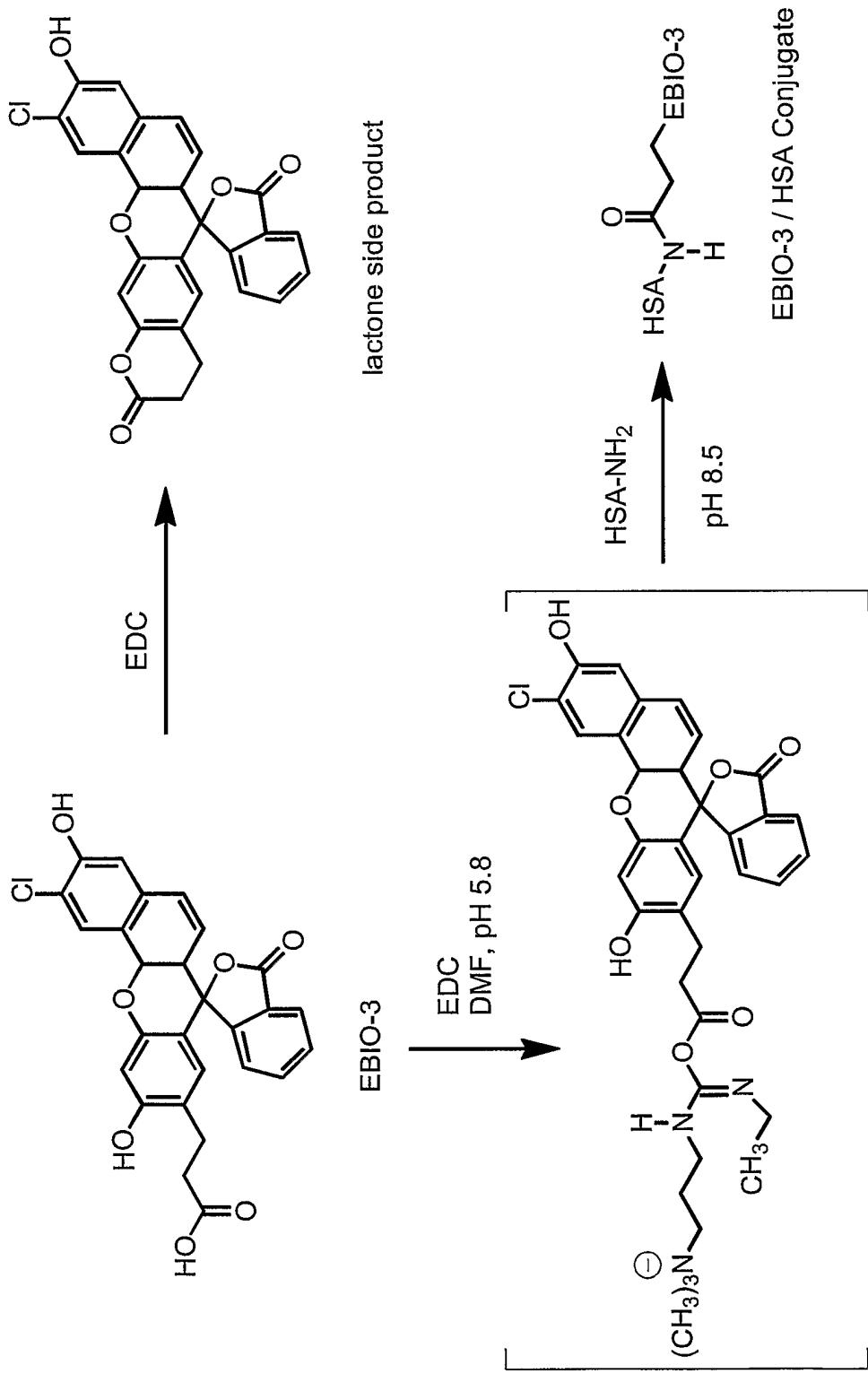


Fig. 10.

12/23

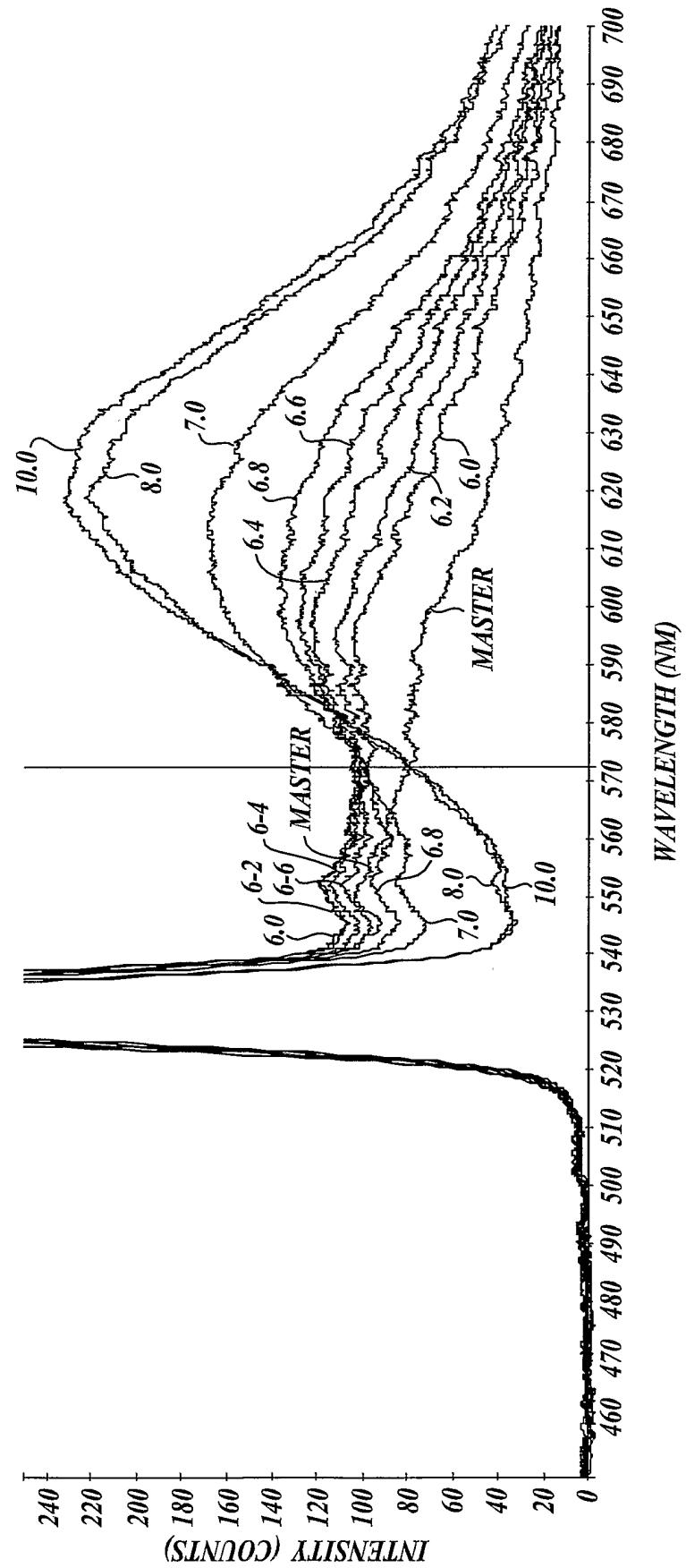


Fig. 11.

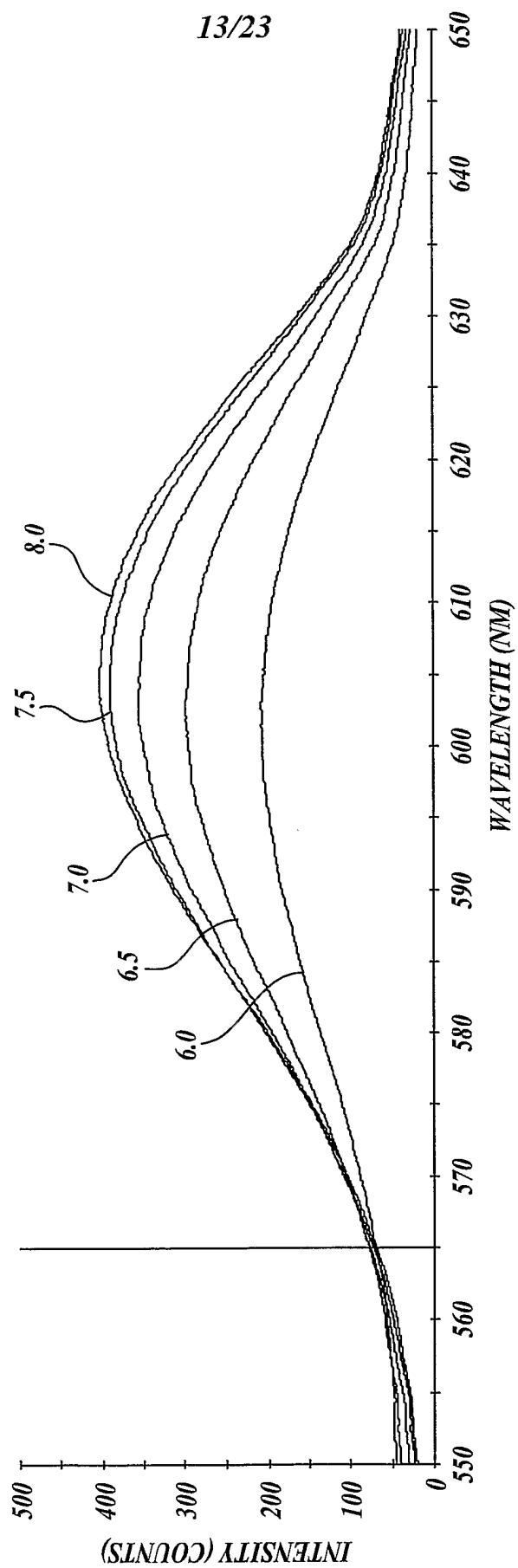


Fig. 12.

14/23

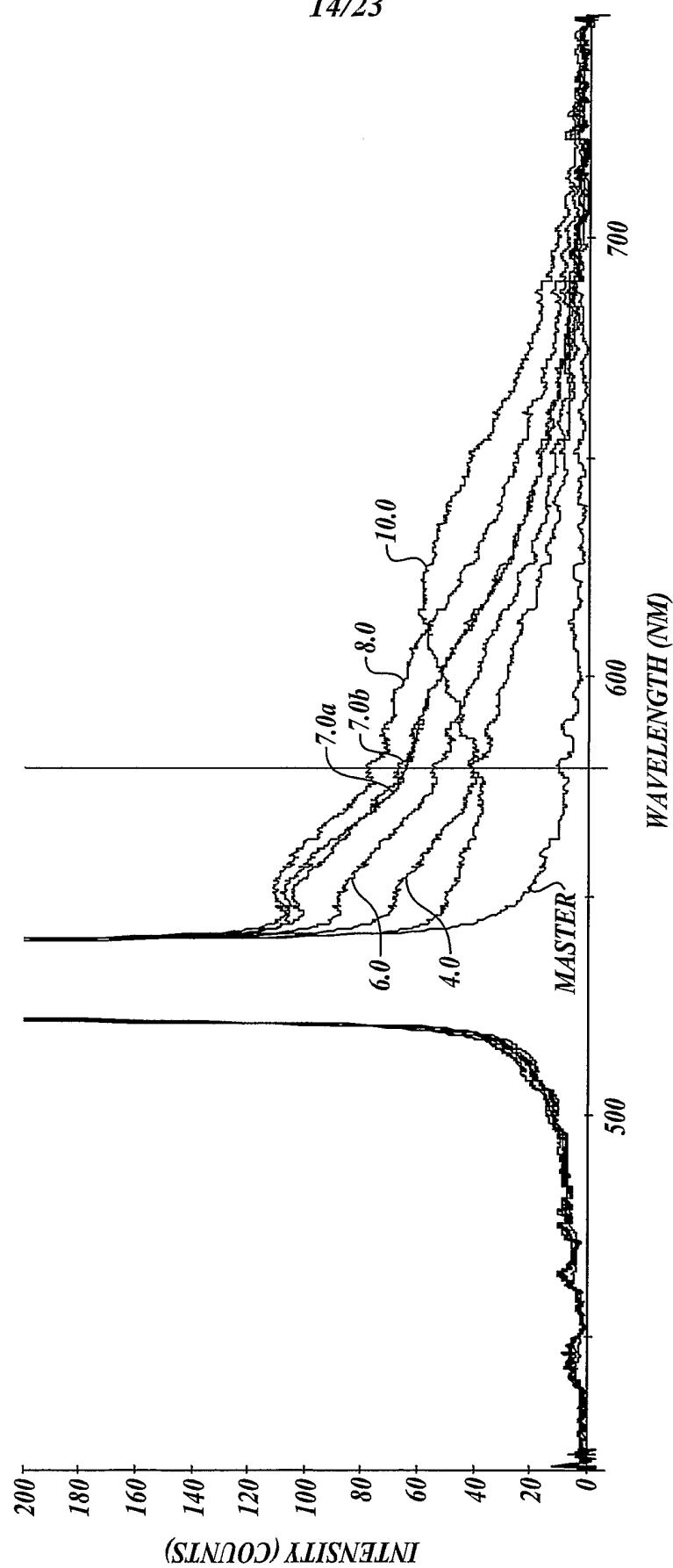


Fig. 13.

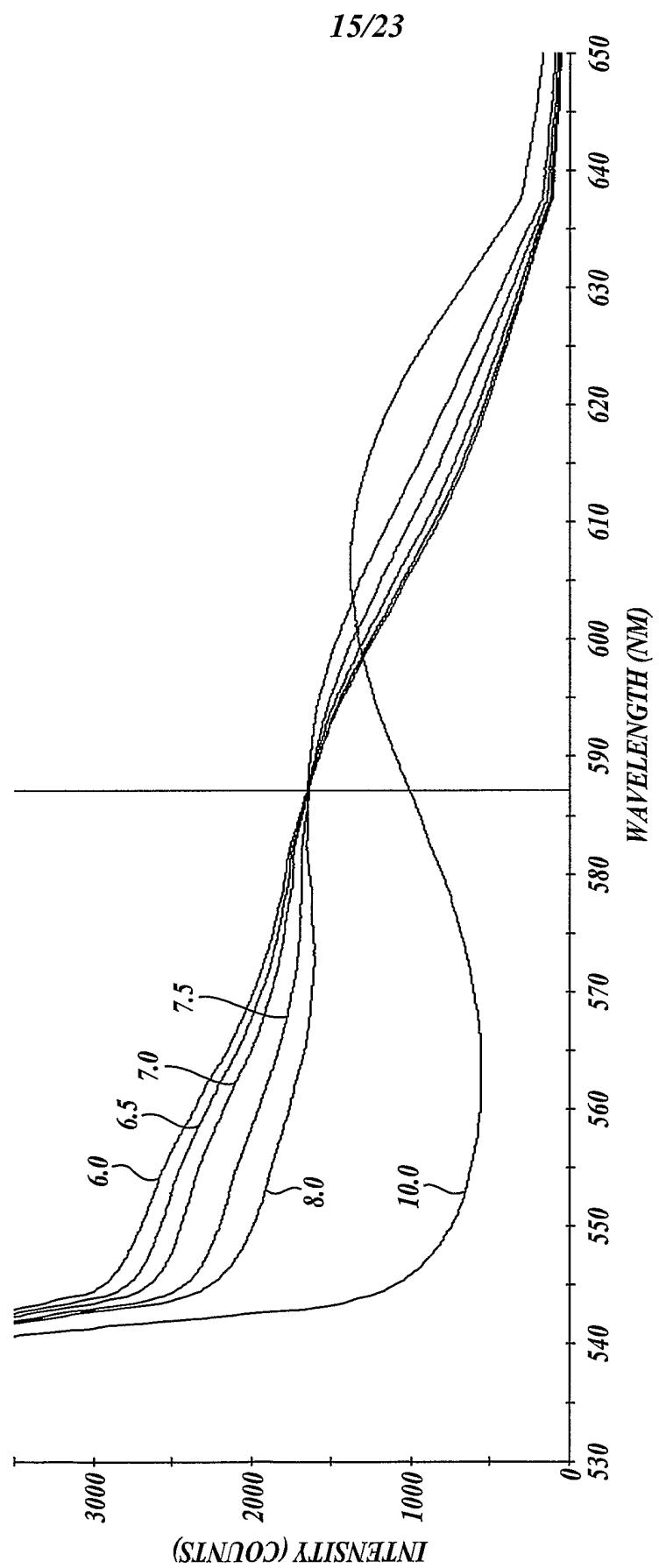


Fig. 14.

16/23

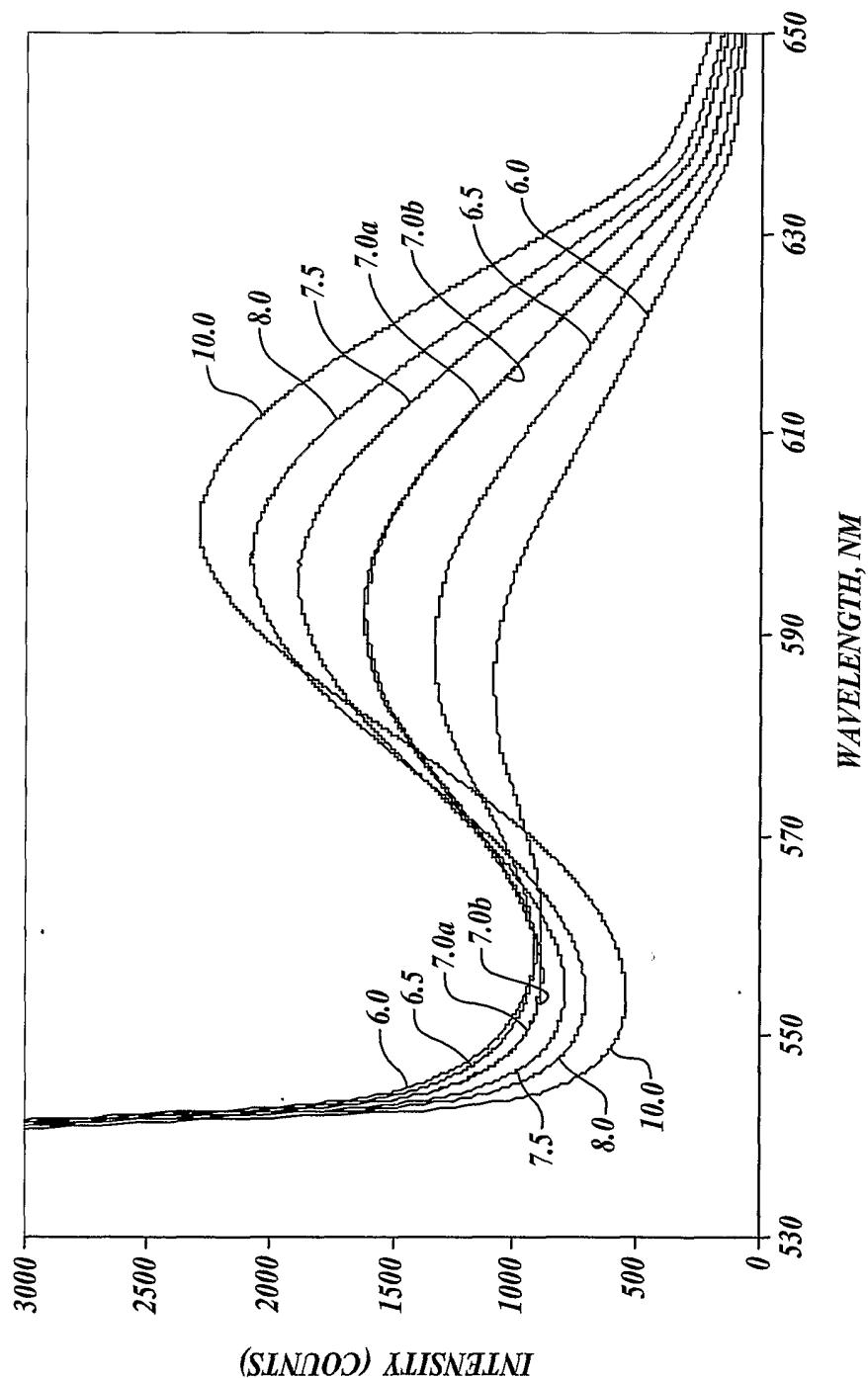


Fig. 15.

17/23

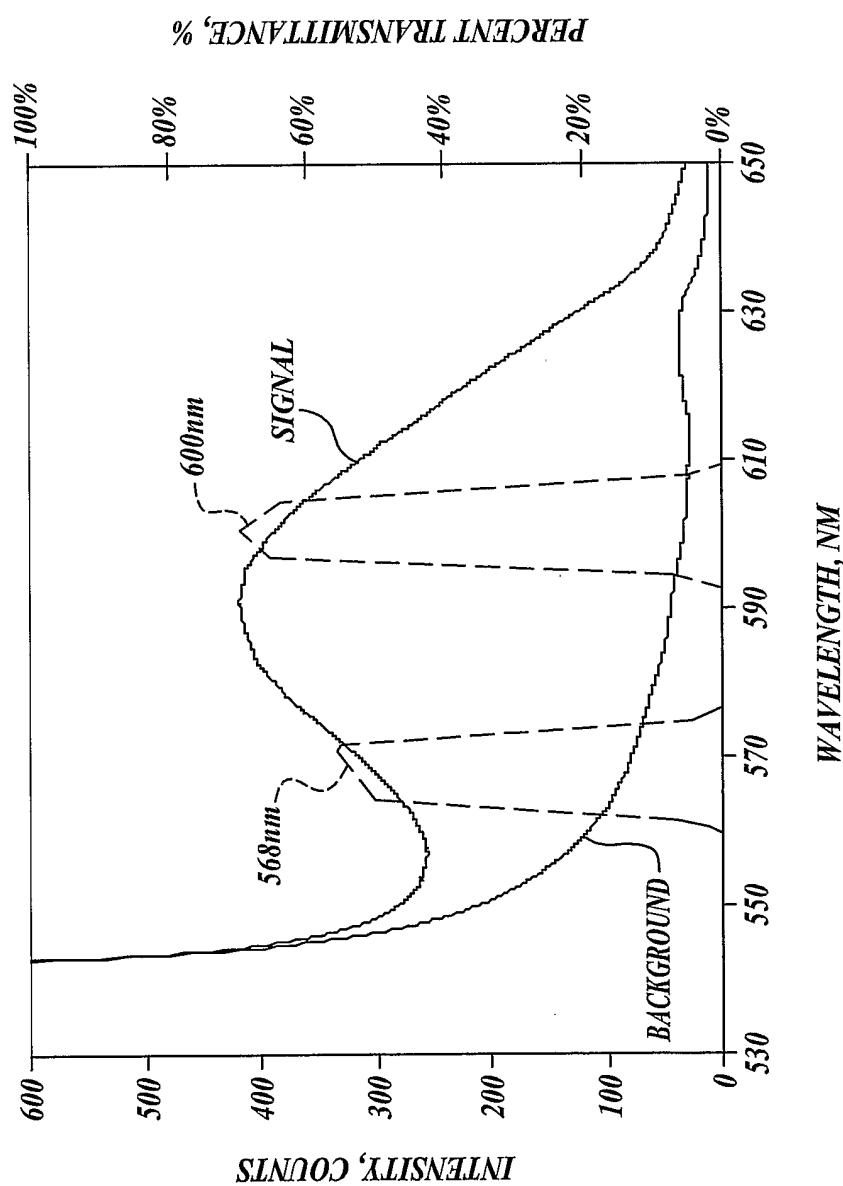


Fig. 16.

18/23

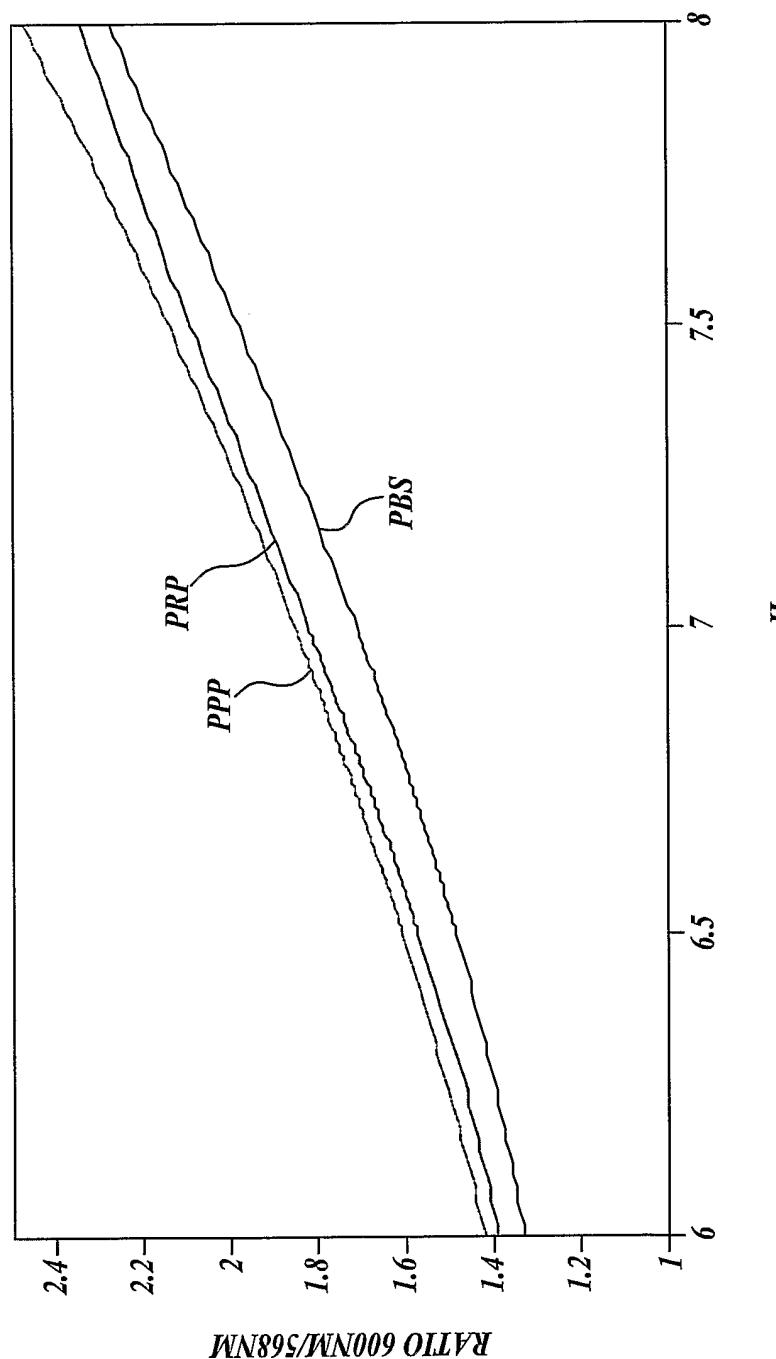


Fig. 17.

19/23

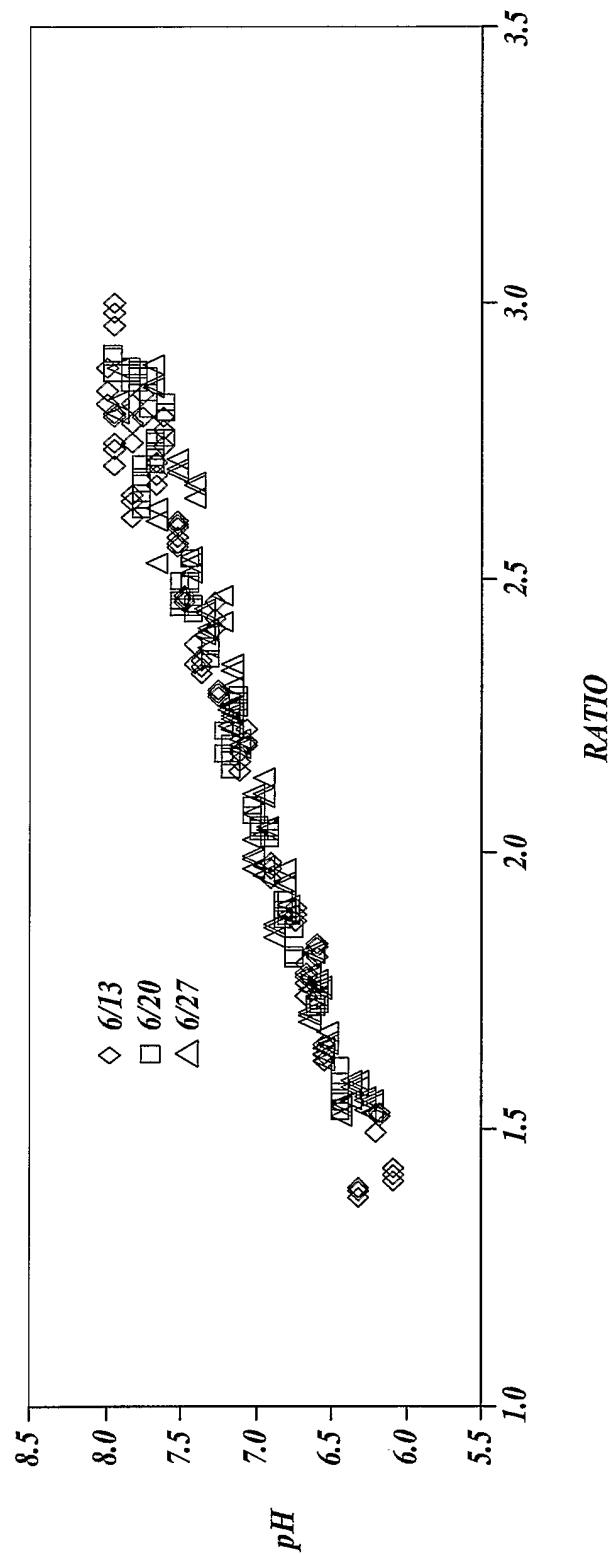


Fig. 18.

20/23

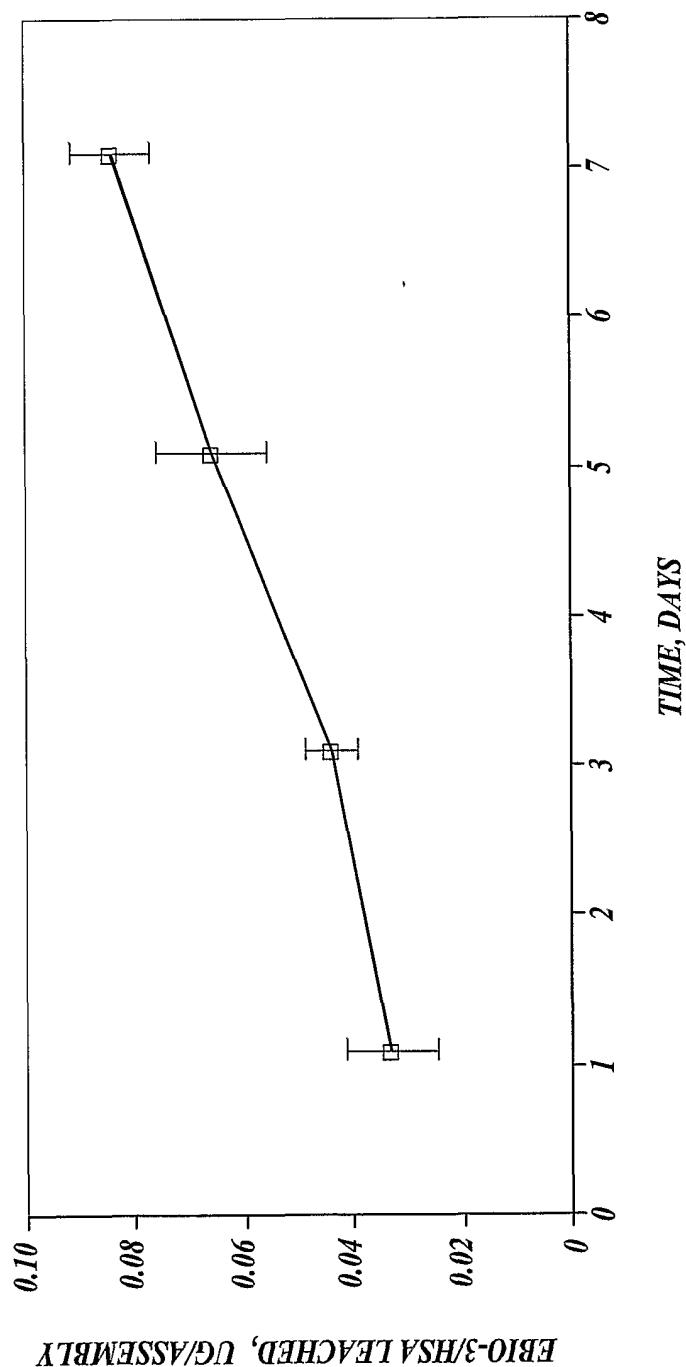
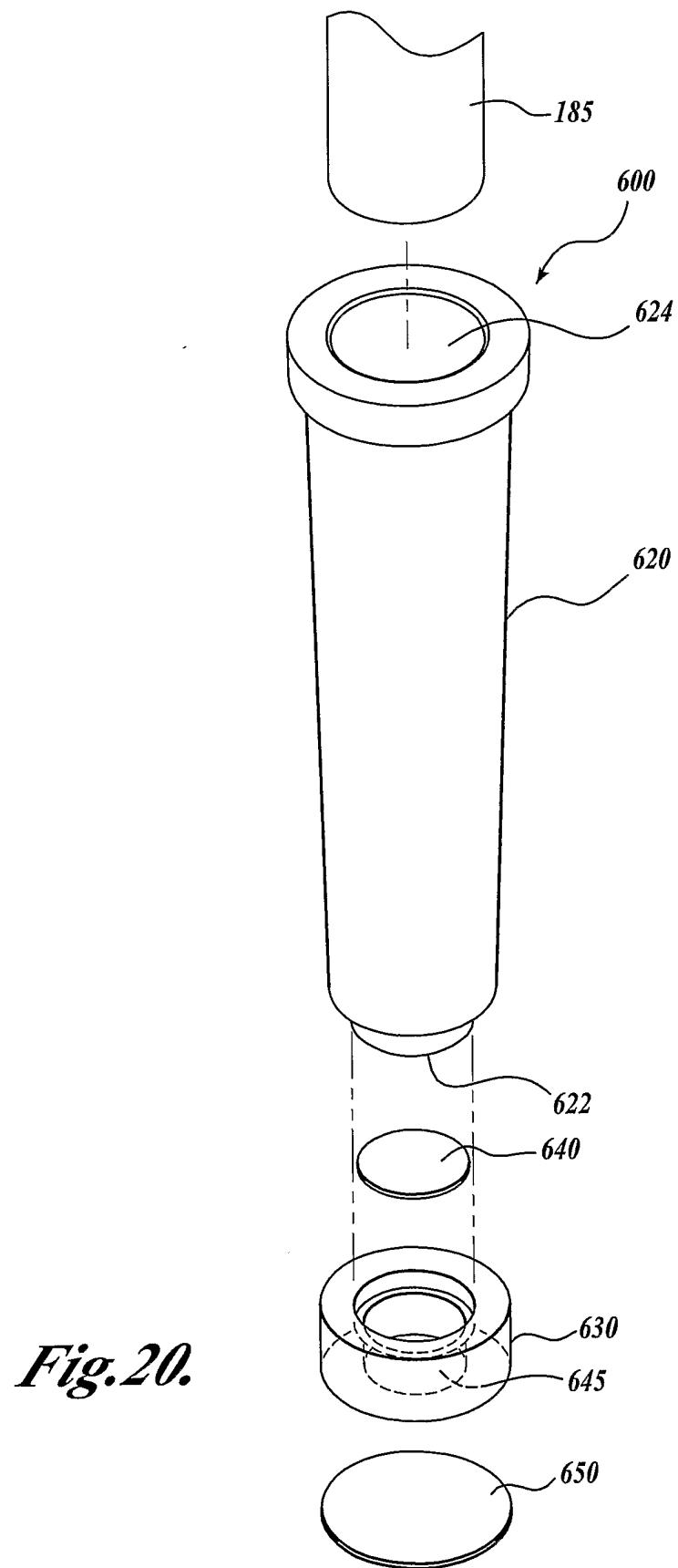


Fig.19.

21/23



22/23

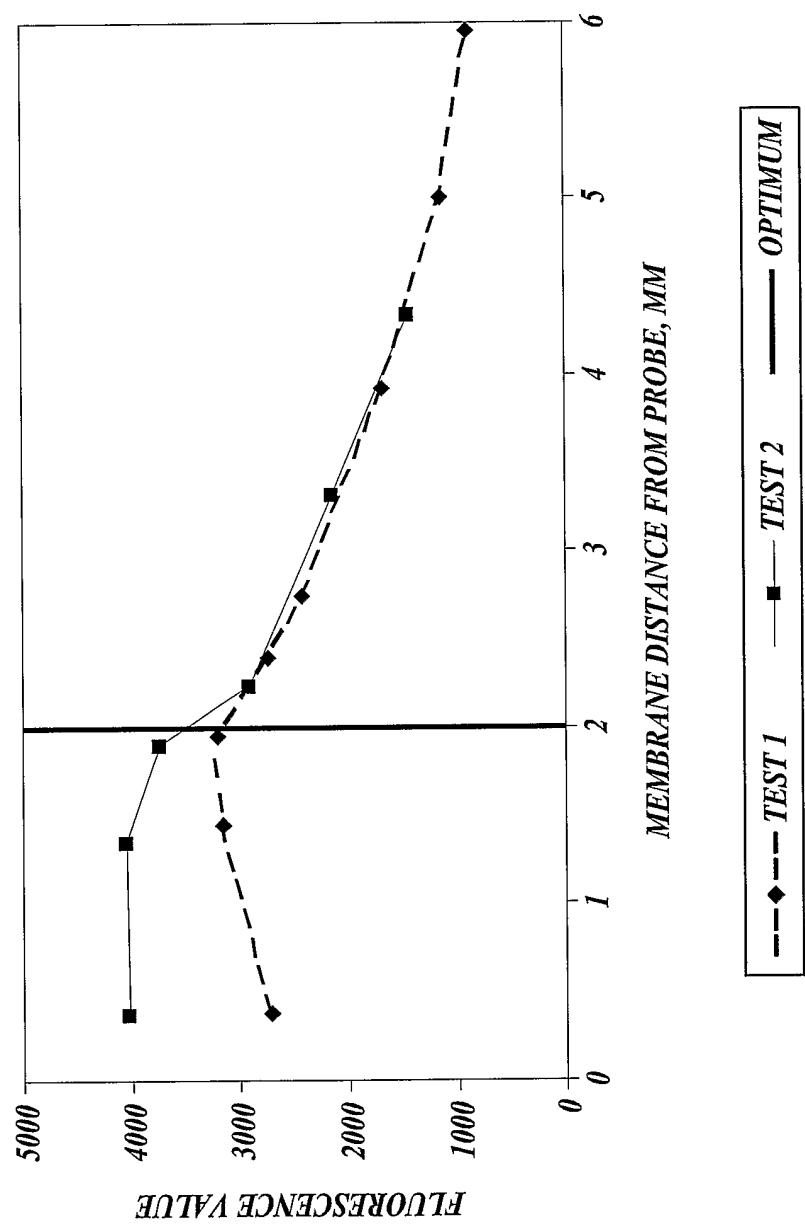


Fig. 21.

23/23

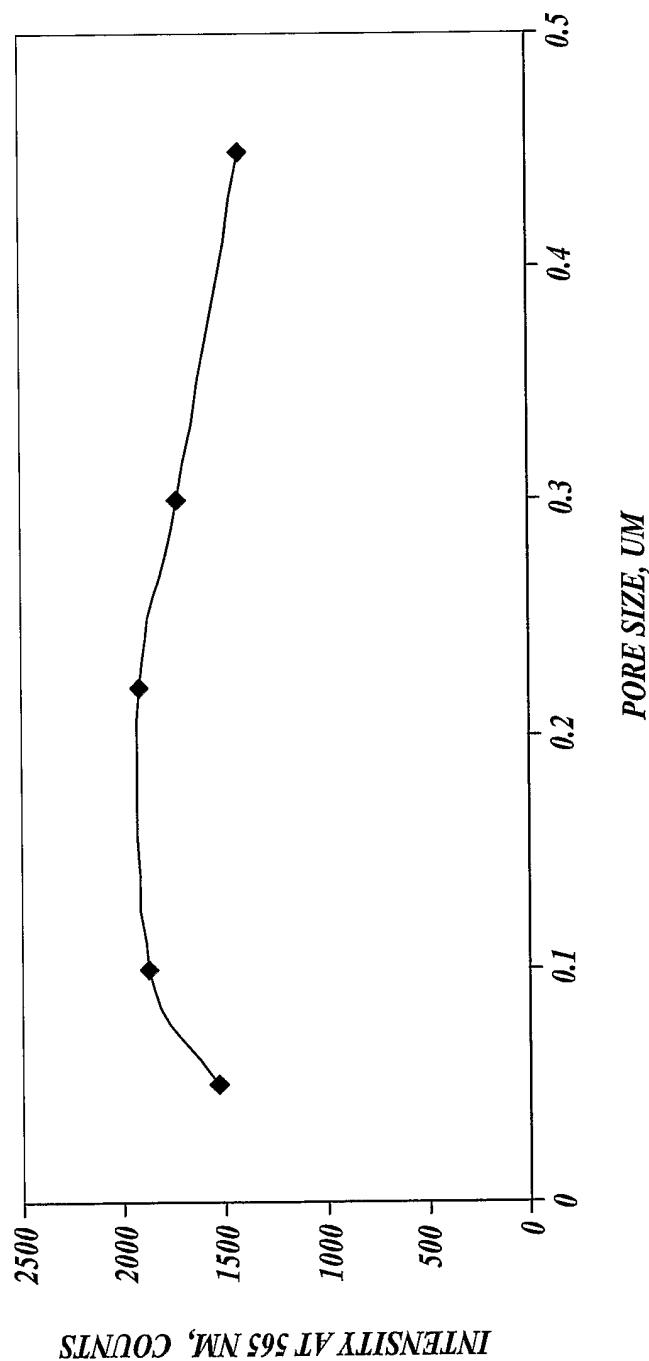


Fig. 22.