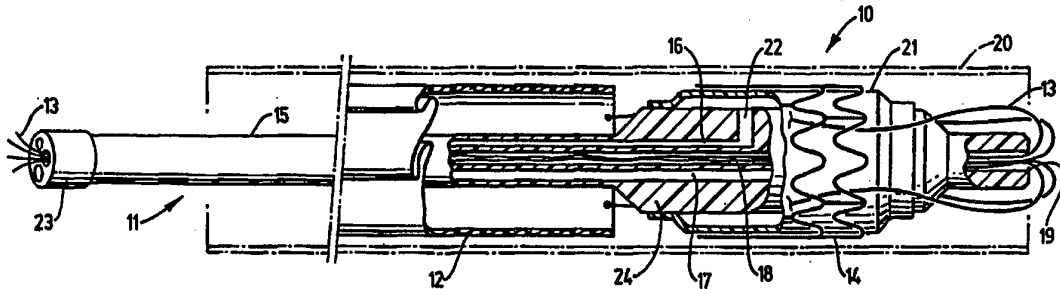




## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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<p>(21) International Application Number: PCT/US96/09149</p> <p>(22) International Filing Date: 5 June 1996 (05.06.96)</p> <p>(30) Priority Data: 08/472,700 6 June 1995 (06.06.95) US</p> <p>(71) Applicant: DEVICES FOR VASCULAR INTERVENTION, INC. [US/US]; 3200 Lakeside Drive, Santa Clara, CA 95052 (US).</p> <p>(72) Inventor: ORTH, Geoffrey, A.; 246 Columbus Street, El Granada, CA 94018 (US).</p> <p>(74) Agents: KOENIG, Nathan, P.; Crosby, Heafey, Roach &amp; May, 1999 Harrison Street, Oakland, CA 94612 (US) et al.</p>		<p>(81) Designated States: CA, JP, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).</p> <p><b>Published</b> <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i></p>

(54) Title: PROSTHETIC GRAFT AND METHOD FOR ANEURYSM REPAIR



## (57) Abstract

This invention provides a method and graft system for aneurysm repair comprising a prosthetic graft with means to draw a distal extremity of the graft over a portion of an expandable anchoring member. Prior to deployment, the graft and the anchoring member do not overlap to reduce the outer diameter of the delivery system. Preferably, the drawing means comprises pull strands connected to the distal extremity of the graft so that the distal extremity of the graft may be pulled over a proximal portion of the anchoring member. Subsequent expansion of the anchoring member seals the overlapped graft against the vessel wall to minimize blood flow-by and secures the graft in the vessel. Securing means may be advanced up each pull strand to abut the anchoring member and further secure the graft to the anchoring member. The graft may also comprise means to guide a second expandable anchoring member to the proximal end of the graft. Preferably, the guiding means comprise guide strands connected to a proximal extremity of the graft. The anchoring member can then be advanced up the guide strands until the graft overlaps the second anchoring member. Expansion of the second anchoring member secures the proximal end of the graft.

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**PROSTHETIC GRAFT AND METHOD  
FOR ANEURYSM REPAIR**

**BACKGROUND**

5 This invention relates to the delivery and placement of vascular  
grafts, and in particular, to a method and system for the repair of  
abdominal aortic aneurysms.

10 An aneurysm is a sac resulting from abnormal dilation of the artery  
wall and is often associated with arteriosclerotic disease. Unless  
treated, an aneurysm can rupture, leading to severe and often fatal  
hemorrhaging. Treating an aortic aneurysm generally involves  
transplanting a prosthetic graft to bridge the affected section of the  
aorta. Surgical implantation of the graft is possible but this treatment  
causes considerable trauma, results in high mortality and morbidity and,  
even when completely successful, requires a lengthy recuperation period.  
15 Due to the difficulty of the operation, direct surgical replacement is even  
less attractive when it must be performed on an emergency basis after  
the aneurysm has ruptured.

20 A less invasive alternative involves the use of a catheter to effect  
intraluminal delivery of a graft. Prior art graft delivery systems, such as  
disclosed in EP 0 461 791 A1 (Barone et al.), employ a graft with  
expandable portions that anchor the graft in the aorta. Often, the  
systems use an inflatable balloon on the delivery catheter to expand the  
anchoring portion of the graft as disclosed in United States Pat. No.  
5,275,622 (Lazarus et al.) which is hereby incorporated in its entirety by  
25 reference thereto. This latter example requires the use of a bulky  
capsule to store the graft and a complicated pushrod system to deploy  
the graft.

Although the referenced prior art systems and others employ many  
different stent and graft configurations, none are completely

satisfactory. The principle limitation of the prior art systems is their size. They typically require a delivery catheter having a diameter of approximately 24-28 French (8 to 9.3 mm). Although it is desirable to introduce grafts through the femoral artery, its inner diameter is only  
5 about 4 to 6 mm. Thus, the size of the prior art devices restricts them to introduction through upper femoral sites, where access may be difficult. Accordingly, there is a need for a graft system capable of introduction through a smaller opening while maintaining the ability to reliably and securely deploy the graft.

10 The success of a percutaneous vessel repair depends in large part on getting the graft to the location of the vasculature in need of repair and deploying the graft effectively. Another difficulty associated with prior art graft deployment systems is blood flow-by which occurs when blood can pass between the graft and the patient's vessel, bypassing the  
15 graft. There is a need for a graft system which minimizes or prevents flow-by.

### **SUMMARY OF THE INVENTION**

This invention provides a method and graft system for aneurysm repair which generally comprises a prosthetic graft with means to draw a  
20 distal extremity of the graft over a portion of an expandable anchoring member. For deployment, the graft and the anchoring member are radially compressed and positioned adjacent one another coaxially on a delivery catheter with essentially no overlap between the distal end of the graft and the proximal end of the anchoring member. The drawing  
25 means is connected to the distal extremity of the graft so that when tension is applied to the graft by the drawing means, the distal extremity of the graft is caused to overlap a proximal portion of the anchoring member. Subsequent expansion of the anchoring member seals the overlapped graft against the vessel wall to minimize blood flow-by and

secures the graft in the vessel. Since the graft and anchoring member do not overlap when loaded on the catheter prior to deployment, the system maintains an overall low profile.

5 In a preferred embodiment, the drawing means comprises at least one and preferably four pull strands attached to the distal end of the graft. The pull strands extend outside the distal end of the catheter, are threaded through an opening at the distal end of the delivery catheter and extend through a lumen in the catheter to the proximal end. After the graft is properly positioned within a patient's vasculature, tension is applied to the pull strands to cause the graft to slide distally along the catheter until the distal end of the graft extends over the proximal end of the anchoring member. Subsequent expansion of the anchoring member expands the graft, anchors it against the vessel wall and seals the graft against the vessel wall to minimize blood flow-by. Securing means may be advanced up the pull strand to abut the anchoring member and further secure the graft to the anchoring member.

15 The graft may also comprise means to guide a second expandable anchoring member to the proximal end of the graft. The guiding means are connected to a proximal extremity of the graft. In one embodiment, the guiding means comprises at least one and preferably four guide strands. After the distal end of the graft is anchored within the patient's vasculature, the guide strands are laced through the second anchoring member. The anchoring member can then be advanced up the guide strands until it is adjacent the proximal end of the graft. The graft overlaps the second anchoring member and expansion of the anchoring member secures the proximal end of the graft. Preferably, securing means secure the proximal end of the graft to the second anchoring member as described above regarding the drawing means.

### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a sectional elevation of a delivery catheter and graft system embodying features of this invention.

5 FIG. 2 is an elevational view of a distal portion of a delivery catheter and graft system of the invention comprising a self-expanding stent.

FIG. 3 shows an embodiment of the invention comprising pull strand securing means.

10 FIG. 4 illustrates an embodiment of the invention comprising guiding means and downstream graft anchoring.

### DETAILED DESCRIPTION OF THE INVENTION

FIG. 1 is a elevational view, in section, illustrating a catheter system 10 embodying features of the invention which generally comprises a catheter 11 with an aortic graft 12 having drawing means, a plurality of pull strands 13, attached to the distal end and an expandable anchoring member, stent 14, loaded for delivery. The catheter 11 comprises a flexible catheter shaft 15 with proximal and distal ends, an inflation lumen 16, a guidewire lumen 17 and a pull strands lumen 18. Pull strands 13 extend from graft 12, enter the pull strands lumen 18 through opening 19 at the distal end of catheter 11 and exit from the proximal end of catheter 11. Preferably, pull strands 13 may be laced through stent 14 at a point corresponding to the amount of overlap desired. In a preferred embodiment, graft 12 overlaps about half the length of stent 14 prior to expansion. A thin-walled retractable sheath 20 is slidably disposed over the catheter 11 and configured so that it covers the stent 14 and graft 13 during introduction and placement of the catheter system 10 and may be withdrawn once they are in an appropriate position within the patient. In the embodiment of FIG. 1, the

catheter 11 includes an inflatable balloon 21 in fluid communication with the inflation lumen 15 through inflation passage 22 which is configured to expand stent 14. The proximal end of catheter shaft 15 can have a cap 23 bonded to the end to provide access to inflation lumen 16, 5 guidewire lumen 17 and pull strands lumen 18. The configuration of cap 23 allows it to mate in a conventional manner with a multi-arm adaptor (not shown) that supplies inflation fluid and allows guidewire control and manipulation of the pull strands. Cap 23 is preferably formed from metal, although other materials such as plastics are suitable. The 10 diameter of cap 23 allows the compressed graft 12 and stent 14 to be threaded over the proximal end of catheter shaft 14. In a preferred embodiment, catheter shaft 15 has an increased diameter delivery base 24 under balloon 21. The delivery base 24 provides support for the expansion of stent 14 while allowing the remainder of the catheter shaft 15 to have a relatively small diameter. Further details regarding the 15 design of suitable catheters as well as graft and stent materials may be found in the application Serial No. 08/336,875, filed November 9, 1994, which is hereby incorporated in its entirety by reference.

Preferably, the stent 14 is a Bronco<sup>®</sup> stent, available from 20 Advanced Cardiovascular Systems, Inc. of Santa Clara, CA. Alternatively, stent 14 may be self-expanding as shown in FIG. 2. For example, stent 14 may be constructed from shape-memory materials causing it to revert to its expanded shape at body temperatures. In such 25 embodiments, thin-walled sheath 20 would restrain stent 14 until properly positioned. Other suitable means for expanding the stent may be used.

The effective wall thickness of stent 14 does not change between the pre-expanded and expanded states. On the other hand, the graft 12 30 bunches when compressed to conform to the catheter shaft 15 and forms overlaps and pleats, effectively increasing its wall thickness.

Stent 14 and graft 12 are coaxially threaded over the catheter 11; the relatively thick compressed graft 12 is positioned solely over the relatively small diameter catheter shaft 15 while the stent 14 receives the increased support for expansion provided by larger diameter delivery base 24. The lack of overlap between the graft 12 and the stent 14 when loaded for deployment on catheter shaft 15 saves approximately 1-3 mm from the diameter of system 10 over conventional systems. Accordingly, the delivery catheters of this invention have an insertion diameter of less than 7 mm and preferably about 6 mm. This allows system 10 to present a small outer diameter to facilitate introduction into the body, preferably through the femoral artery.

In embodiments where pull strands 13 are laced through stent 14, securing means 25 may be employed to further anchor the graft 12 as shown in FIG. 3. The securing means 25 thread over pull strands 13 and are configured so that they will not pass through the framework of stent 14. In one embodiment, securing means 25 comprise one-way frictional sliding washers. Once graft 12 and stent 14 are deployed and catheter 11 removed, a simple catheter 26 is used to push securing means 25 up pull strands 13 until they are tightly seated against stent 14. This secures pull strands 13 to stent 14 and further anchors the graft 12.

FIG. 4 illustrates an embodiment of the invention which comprises guiding means, guide strands 27, attached to the proximal end of graft 12. Guide strands 27 are similar in configuration to pull strands 13. In use, the graft's distal end (or ends in the case of a bifurcated graft) 12 may be anchored by lacing guide strands 27 through a second anchoring member, stent 28, and advancing the stent 28 up the guide strands until it is at least immediately adjacent to the proximal end of graft 12. Once positioned, the anchoring member 28 is expanded to secure the proximal end of graft 12 and maintain the graft's patency. Securing means 25 may be used to further anchor the graft as described above. In some



embodiments, the guide strands **27** are attached to the interior of graft **12** at a point inset from the proximal end to allow that proximal portion of graft **12** to overlap a distal portion of stent **28** such that expansion of stent **28** will sandwich the proximal end of the graft against the patient's vessel wall.

In general, anchoring members may be formed from any suitable material, including tantalum, stainless steel, other metals and polymers and when employing a self-expanding anchoring member, shape-memory metals such as NiTi alloys. The anchoring member may also be coated with a polymer or seeded with endothelial cells to further inhibit thrombosis. Generally, the anchoring member is formed in its pre-expanded state. Once it is positioned with the graft over the catheter shaft **15**, the anchoring member may be crimped down to a slightly smaller inner diameter onto the means for expanding the anchoring member to secure the assembly during introduction and to further reduce the delivery diameter. Anchoring member configurations are suitable so long as they are self supporting within the aortic passageway and provide suitable means for anchoring the graft.

The grafts of this invention are intact tubes, preferably constructed of a synthetic yarn, monofilament or multifilament, formed from materials such as polyesters (including Dacron®), polytetrafluoroethylene (PTFE), polyurethane or nylon. Dacron® in particular, a multifilament composed of polyethylene terephthalate (PET), has been shown to be suitable and may promote formation of intima. The synthetic material may be woven or knit. The woven grafts are generally stronger and less porous while knit grafts are softer and more porous. Additionally, the surface of the synthetic material may be texturized and woven or knit to form a velour surface which generally facilitates growth of tissue from the surrounding lumen through the velour loops to help secure the graft. If desirable, the graft may be

bifurcated.

The catheter **11** may be formed from any suitably flexible material, such as pseudoelastic metals (*e.g.* NiTi alloys) and a wide range of conventional polymers. Preferably, the catheter **11** is formed from an extrudable polymer such as polyethylene (PE).

The inflatable balloon **21** may be a relatively inelastic inflatable balloon to provide the degree of expansion control and durability necessary to effectively expand and anchor the anchoring member. The balloon may be formed from any suitable material such as PE, polyethylene terephthalate (PET) or nylon or other polyamide.

Pull strands **13** and guide strands **27** may comprise any suitable material having sufficient flexibility to easily thread through the anchoring means and the catheter while having sufficient strength to pull the graft over the stent. Suitable materials include plastics and metals. In some embodiments, pull strands **13** and guide strands **27** may comprise integral parts of the graft **12**. It may be desirable to form all or a portion of pull strands **13** and guide strands **27** from a bioabsorbable material. It is preferable to provide the graft **12** with four pull strands **13** and four guiding strands **27**, each radially spaced around the respective end of the graft.

The use of the catheter system **10** generally follows conventional procedures. In particular, a guidewire (not shown) is backloaded into guidewire receiving lumen **17** of the catheter **11** with sheath **20** extending over the compressed and loaded graft **12** and stent **14**, as shown in phantom. The catheter system **11** and guidewire are percutaneously introduced by means of conventional cut down techniques in the patient's arterial system, generally through the femoral artery. The guidewire is advanced out delivery catheter **11** and up the aorta via fluoroscopic imaging until it crosses the aneurysm. Then the catheter **11** is advanced over the guidewire until the stent **14** is

positioned within a healthy region of the aorta upstream from the aneurysm. The sheath **20** is retracted to expose the stent **14** and the graft **12**. Pull strands **13** are pulled to draw the distal end of the graft a desired amount over the proximal end of the stent **14**, preferably half the length of the stent. Then, balloon **21** is inflated to expand stent **14** to sandwich the distal end of graft **12** between the stent **14** and the aortic wall, thus anchoring it. The balloon **21** is deflated and the catheter **11** is removed, leaving the expanded anchoring member and graft in place. To further secure the graft, securing means **25** may be advanced up pull strands **13** until they abut the stent **14**. Once securing means **25**, if any, are positioned, all excess of the pull strands **13** may be cut.

Once deployed, the proximal end or ends of graft **12** may be anchored by advancing another anchoring member **28** along guide strands **27**. Securing means **25** may also be employed to further anchor the proximal end of graft **12** to anchoring member **28**.

While the invention has been described primarily with respect to a system comprising the catheter loaded with an anchoring member and graft, it includes the graft with drawing means alone, kits which comprise unassembled catheters, anchoring members and grafts, and methods of use. It should be recognized that various modifications and improvements can be made to the invention without departing from the scope thereof.

What is claimed is:

1. A graft delivery system comprising:
  - a) an elongated catheter with proximal and distal ends and a means for expanding an expandable anchoring member on a distal portion of the catheter;
  - b) an expandable anchoring member with proximal and distal ends mounted on the expanding means;
  - c) an aortic graft in a radially compressed state with proximal and distal ends and mounted on the catheter proximally adjacent to the anchoring member; and
  - d) drawing means secured to the distal end of the graft and configured to pull the distal end of the graft over the proximal end of the anchoring member.
2. The graft delivery system of claim 1 wherein the catheter further comprises a lumen with a opening at the distal end and extending to the proximal end and the drawing means comprises at least one pull strand extending from the distal end of the graft through the opening at the distal end of the catheter to the proximal end of the catheter.
3. The graft delivery system of claim 2 wherein the pull strands are laced through the anchoring member.
4. The graft delivery system of claim 1 wherein the means for expanding an anchoring member comprises an inflatable member.
5. The graft delivery system of claim 4 including an inflation lumen extending through the catheter in fluid communication with the

interior of the inflatable member.

6. The graft delivery system of claim 1 wherein the system has an outer diameter of less than about 7 mm.

5 7. The graft delivery system of claim 1 wherein the anchoring member comprises a stent.

8. The graft delivery system of claim 1 wherein the graft further comprises guiding means extending from the proximal end of the graft.

10 9. The graft delivery system of claim 8 wherein the guiding means comprise at least one guiding strand.

10. A graft delivery system comprising:

- 15 a) an elongated catheter with proximal and distal ends;  
b) a self-expanding anchoring member with proximal and distal ends mounted on a distal portion of the catheter;  
c) an aortic graft in a radially compressed state with proximal and distal ends and mounted on the catheter proximally adjacent to the anchoring member; and  
20 d) drawing means secured to the distal end of the graft and configured to pull the distal end of the graft over the proximal end of the anchoring member.

11. The graft delivery system of claim 10 wherein the catheter further comprises a lumen with a opening at the distal end and extending to the proximal end and the drawing means comprise pull strands extending from the distal end of the graft through the opening at the

distal end of the catheter to the proximal end of the catheter.

12. The graft delivery system of claim 11 wherein the pull strands are laced through the anchoring member.

5 13. The graft delivery system of claim 10 wherein the self-expanding anchoring member is formed from shape-memory material.

14. The graft delivery system of claim 13 wherein the anchoring member is formed from a NiTi alloy.

10 15. The graft delivery system of claim 10 wherein the graft further comprises guiding means extending from the proximal end of the graft.

16. The graft delivery system of claim 15 wherein the guiding means comprise at least one guiding strand.

17. An aortic graft comprising a graft having proximal and distal ends with drawing means attached to the distal end.

15 18. The graft of claim 17 wherein the drawing means comprises at least one pull strand.

19. The graft of claim 17 wherein the graft further comprises guiding means extending from the proximal end of the graft.

20 20. The graft of claim 19 wherein the guiding means comprises at least one guiding strand.

21. A method for repairing a portion of a patient's vasculature comprising the steps of:

a) providing a catheter assembly having:

1) an elongated catheter with proximal and distal ends and a means for expanding an expandable anchoring member on a distal portion of the catheter,

2) an expandable anchoring member with proximal and distal ends mounted on the expanding means,

3) an aortic graft in a radially compressed state with proximal and distal ends and mounted on the catheter proximally adjacent to the anchoring member, and

4) drawing means secured to the distal end of the graft and configured to pull the distal end of the graft over the proximal end of the anchoring member; and

b) advancing the catheter assembly with the graft to the desired location in the patient's vasculature;

c) operating the drawing means to pull the distal end of the graft over the proximal end of the anchoring member; and

c) expanding the anchoring member to expand and anchor the graft within the patient's vasculature.

22. The method for repairing a portion of a patient's vasculature of claim 21 further comprising the step of attaching securing means on drawing means abutting the anchoring means to anchor the graft.

23. The method for repairing a portion of a patient's vasculature of claim 21 wherein the graft further comprises guiding means and further comprising the steps of:

a) lacing the guiding means through a second anchoring member;

b) advancing the second anchoring member along the guiding means through the patient's vasculature until it is at least adjacent to the proximal end of the graft; and

c) expanding the second anchoring member to anchor the proximal end of the graft.

24. A method for repairing a portion of a patient's vasculature comprising the steps of:

a) providing a catheter assembly having:

1) an elongated catheter with proximal and distal ends,

2) a self-expanding anchoring member with proximal and distal ends mounted on a distal portion of the catheter,

3) an aortic graft in a radially compressed state with proximal and distal ends and mounted on the catheter proximally adjacent to the anchoring member, and

4) drawing means secured to the distal end of the graft and configured to pull the distal end of the graft over the proximal end of the anchoring member; and

b) advancing the catheter assembly with the graft to the desired location in the patient's vasculature;

c) operating the drawing means to pull the distal end of the graft over the proximal end of the anchoring member; and

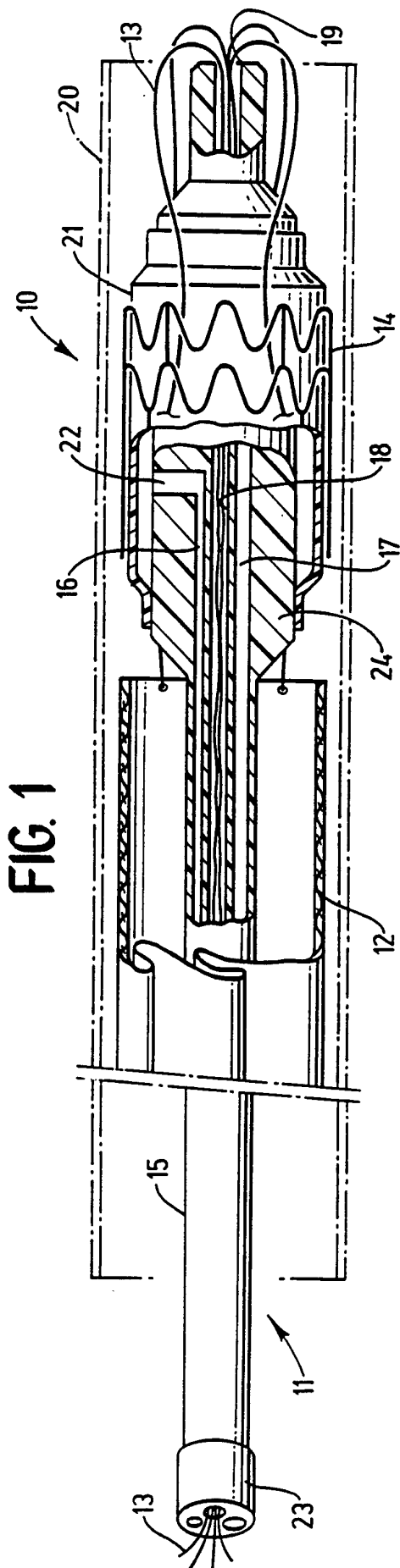
c) allowing the self-expanding the anchoring member to expand and anchor the graft within the patient's vasculature.

25. The method for repairing a portion of a patient's vasculature of claim 24 further comprising the step of attaching securing means on drawing means abutting the anchoring means to anchor the graft.

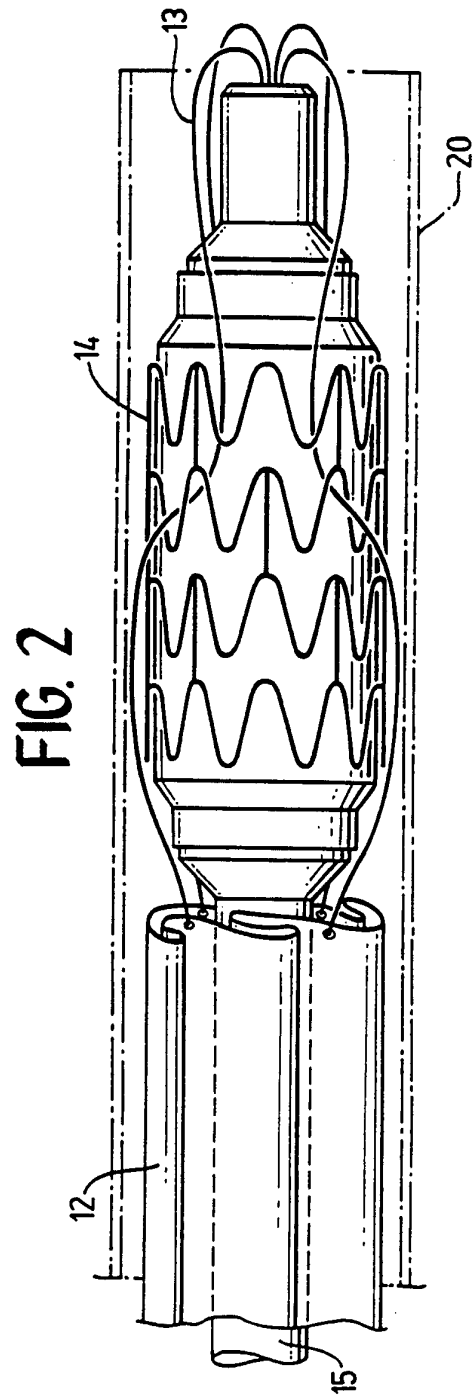


26. The method for repairing a portion of a patient's vasculature of claim 24 wherein the graft further comprises guiding means and further comprising the steps of:

- 5 a) lacing the guiding means through a second anchoring member;
- b) advancing the second anchoring member along the guiding means through the patient's vasculature until it is at least adjacent to the proximal end of the graft; and
- 10 c) expanding the second anchoring member to anchor the proximal end of the graft.



1/2



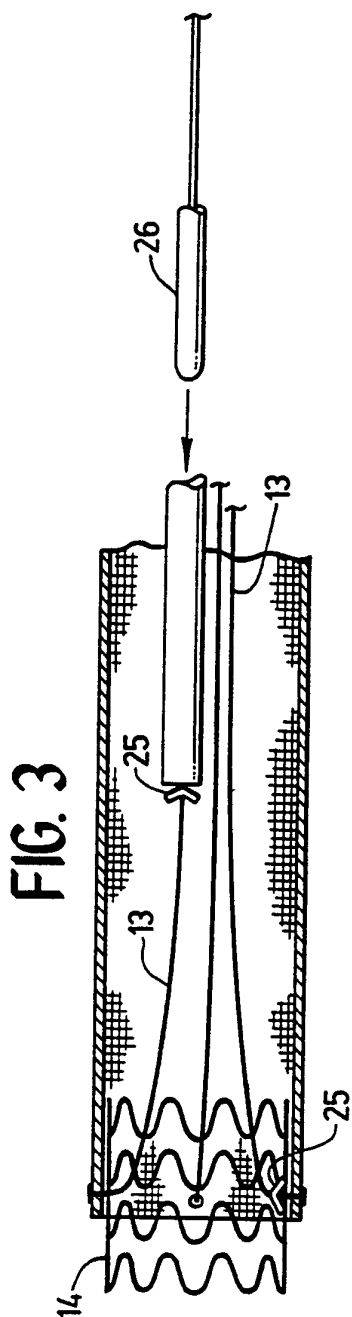


FIG. 3

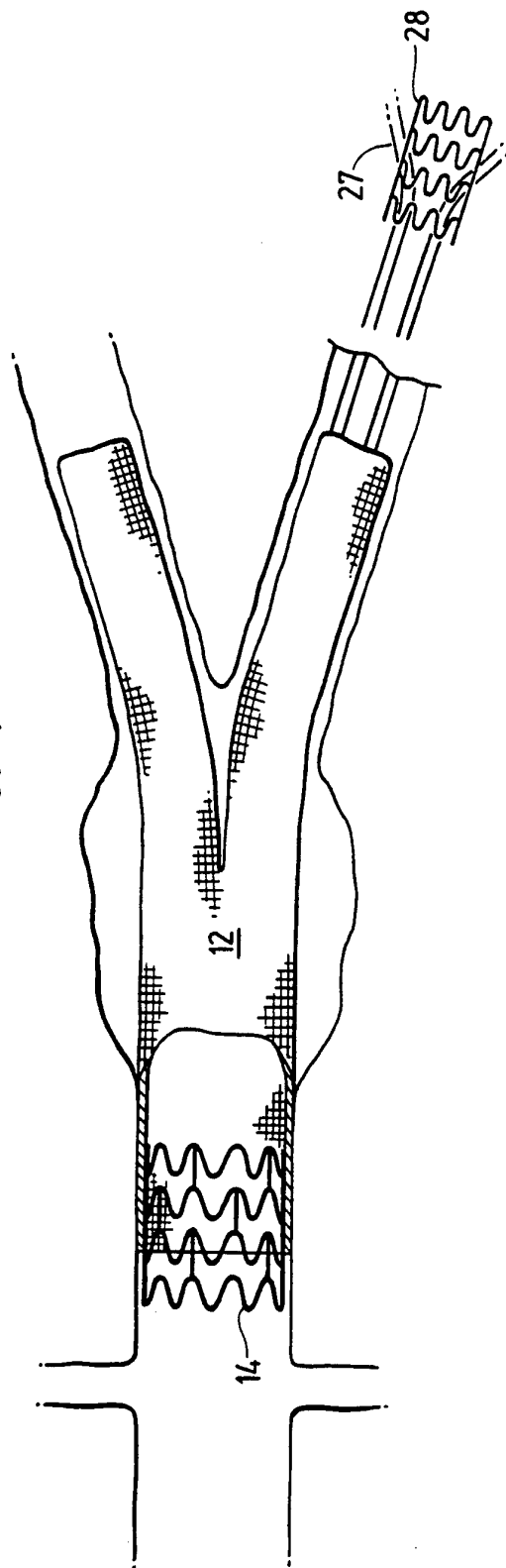


FIG. 4

# INTERNATIONAL SEARCH REPORT

International Application No  
PCT/US 96/09149

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 6 A61F2/06

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X A	EP,A,0 539 237 (COOK INC) 28 April 1993 see column 18, line 4 - line 18; figures	17-20  1,7-10, 15,16
Y A	---	
Y A	EP,A,0 637 454 (ENDOVASCULAR TECH INC) 8 February 1995 see the whole document	17,18  1,4-9
Y A	---	
Y A	EP,A,0 321 912 (DELSANTI GERARD L) 28 June 1989 see abstract; figures	17,18
Y A	---	
Y A	EP,A,0 556 850 (ENDOTECH LTD) 25 August 1993 see column 4, line 42 - line 55; figures	1,7,10, 13,17
Y A	-----	

Further documents are listed in the continuation of box C.

Patent family members are listed in annex.

\* Special categories of cited documents :

- \*A\* document defining the general state of the art which is not considered to be of particular relevance
- \*E\* earlier document but published on or after the international filing date
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- \*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- \*Y\* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
- \*&\* document member of the same patent family

Date of the actual completion of the international search

30 October 1996

Date of mailing of the international search report

06. 11. 96

Name and mailing address of the ISA

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# INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 96/09149

## Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1.  Claims Nos.: 21-26  
because they relate to subject matter not required to be searched by this Authority, namely:  
PCT Rule 39.1(iv)
2.  Claims Nos.:  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3.  Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1.  As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2.  As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3.  As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4.  No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

The additional search fees were accompanied by the applicant's protest.

No protest accompanied the payment of additional search fees.

# INTERNATIONAL SEARCH REPORT

information on patent family members

International Application No

PCT/US 96/09149

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
EP-A-0539237	28-04-93	US-A- 5387235	07-02-95
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		CA-A- 2081424	26-04-93
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		JP-A- 5305092	19-11-93
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		AU-A- 6474794	16-03-95
		CA-A- 2125258	06-02-95
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