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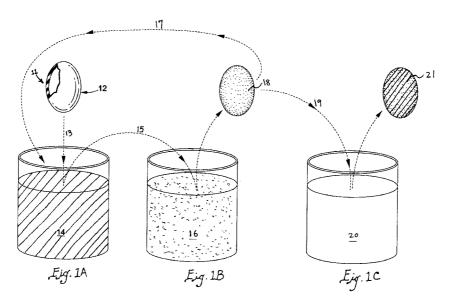
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(57) Abstract: Implantable prosthesis, components of prosthesis, and methods of making same are provided. The methods generally include the steps of providing an implant shell, applying a curable fluid composition to the shell to form a coating thereon and applying a particulate component to the composition. The composition is a mixture, for example, an emulsion, containing a silicone-based elastomer dispersion and droplets of a suspended leachable agent. After the elastomer is stabilized and cured, the particulate component and leachable agent are removed, resulting in an implantable member having a porous, open-cell surface texture designed to be effective in reducing incidence of capsular formation or contraction.





IMPLANTS AND METHODS FOR MANUFACTURING SAME

By Inventors Alexei Goraltchouk, Dennis VanEpps and
Thomas E. Powell

5 Related Application

This application claims priority to U.S. Provisional Patent Application No. 61/252,330, filed on October 16, 2009, the entire disclosure of which is incorporated herein by this specific reference.

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Background

The present invention generally relates to soft tissue implants and more specifically relates to soft tissue implants designed to enhance fixation in the body and/or alter or reduce capsular formation.

Soft tissue implants, particularly mammary prostheses, are plagued by problems of capsular formation and contracture. Soon after an implant is placed into the body, an inflammatory response begins to deposit a fibrous capsule around the implant. In most cases, particularly for relatively large and smooth implants, the capsule is comprised of highly organized or aligned collagen fibers. As the capsule matures, certain events may trigger the differentiation of fibroblasts to a contractile phenotype (myofibroblasts). In this or similar scenarios, and if the collagen fibers are aligned, capsular contracture may ensue.

Capsular contracture can be debilitating to the patient
30 because of discomfort or even pain caused thereby, can
diminish the efficacy of the aesthetic results in both the
look and feel of the implant, and can sometimes damage the
implant itself. Problems with capsular formation and
contracture occur in many implant types such as pacemakers,
35 dura matter substitutes, implantable cardiac defibrillators,

pacemaker leads, hernia repair meshes as well as breast and other esthetic implants.

It has been established in the literature that surface

texturing of implants often helps to reduce the incidence of
capsular contracture when compared to smooth surface
implants. Furthermore there is increasing evidence regarding
the ability of foam covered implants, for example,
polyurethane foam coated implants, to reduce contracture

rates. However, polyurethane foam coatings are
biodegradable and lose their efficacy once the polyurethane
degrades. Further, it can be appreciated that degradation
of polyurethane foam into the body is undesirable and
potentially unhealthy.

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The present invention addresses at least some of these drawbacks of conventional implants.

Summary of the Invention

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The present invention provides implantable members and methods for manufacturing implantable members, for example, prostheses, for example, mammary prostheses, as well as components of prostheses, for example, elastomeric shells, 25 which serve as components of mammary prostheses. The invention further provides coverings, for example, laminates for applying to surfaces of implantable devices. The implantable members have surfaces which may enhance fixation and/or alter or reduce capsular formation. In one aspect of 30 the invention, the textured surfaces are defined by a network of interconnected pores and channels which encourages tissue ingrowth and discourages organization of the collagen capsule. Generally, the pores have, on average, more than two interconnections assuming that the

average number of interconnections per pore does not vary significantly.

The method generally comprises the steps of providing an implantable member, for example an implant shell, for example, a conventional smooth silicone-based implant shell, and applying a curable fluid composition to the shell to form a coating thereon. In one embodiment, the composition comprises a silicone-based mixture including a solvent, and a pore-forming material, for example, a leachable agent, dispersed therein. The composition is allowed to stabilize on the shell, for example, by allowing some of the solvent to evaporate out of the composition or allowing a chemical reaction to occur inducing precipitation of the soluble components. Alternatively, stabilization can be achieved during crosslinking of polymerization of the silicone, precipitation of the silicone or pore-forming material of a combination of the above alone or in conjunction with solvent evaporation.

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Next, a particulate component, hereinafter sometimes simply referred to as "particles" or a "particle coating", is applied to the composition coating while the composition coating is less than entirely cured, or at least has a stickiness or tackiness capable of retaining the particulate coating.

In some embodiments, the steps of applying a curable fluid composition and applying a particle coating are then repeated, for example, one or more times, for example, three, five or even up to 20 times, until a final coating is applied. The final coating may be a particle coating or a composition coating.

After the final coating of particles or fluid composition is applied to the shell, the coated shell is then subjected to suitable curing conditions to solidify the composition with the particles embedded therein.

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In one embodiment, the particulate coating itself is used to stabilize the coating composition, for example, by absorbing some or all of the solvent, increasing the rate of polymerization of crosslinking of the silicone, promoting precipitation of the silicone or porogen, or a combination of one or more of the above.

Once solidified, the leachable agent contained in the composition and the particles embedded therein are then removed from the coating thereby revealing a network of interconnected pores (the structure may include both relatively large pores and relatively smaller pores, for example, micropores) within the cured elastomer. The surface topography created by the processes described herein, when used as a part of an implant at the tissue/implant interface, may be highly effective in altering capsular formation so as to achieve a more preferred morphology, or in reducing or preventing capsular contracture, relative to conventional surface topographies.

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Removal of the particles and leachable agent may be accomplished by any suitable means effective to remove these materials from the surrounding elastomer "matrix", and create the desirable surface topography.

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For example, the particles and/or leachable agent(s) may be extracted by exposing the coating to one or more suitable mediums capable of dissolving, extracting or otherwise removing the particles and/or leachable agent while leaving the cured elastomer matrix generally intact.

Generally, the particles, which are typically larger in size than the dispersed leachable agent, serve to create cavities or pores in the cured elastomer while the dispersed leachable agent serves to create microcavities or micropores which serve as interconnections between the pores. This network of interconnected pores and micropores facilitates tissue ingrowth, encourages better fixation of the implant in the patient, and discourages organization of the fibrous capsule, which may help reduce or prevent capsule formation and contraction.

Brief Description of the Drawings

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- The present invention may be more clearly understood and the aspects and advantages thereof more clearly appreciated with reference to the following detailed description and accompanying drawings of which:
- 20 Figs. 1A-1C represents suitable process steps in a method for manufacturing an elastomeric shell in accordance with an embodiment of the invention;
- Figs. 2-6 are cross-sectional views of components of the shell during various steps of the process for making the shell shown in Figs. 1A-1C.
- Fig. 7 is a simplified flow chart showing steps in a method for manufacturing an implant shell in accordance with an embodiment of the invention.

Detailed Description

Accordingly, implantable composite members and methods for manufacturing such implantable composite members are provided.

In one aspect of the invention, the present invention provides an implantable composite member, hereinafter, typically referred to as an "implant", having a surface that renders the implant effective in reducing the occurrence or severity of capsule formation when the implant is placed in the body. In a specific exemplary embodiment that will now be described, the implant is a fillable mammary prosthesis useful in breast reconstruction or breast augmentation. It should be appreciated, however, that the present invention is not limited to mammary prostheses, but is useful in many situations in which an implant is intended to be permanently or temporarily placed in the body and which capsule formation or contraction is to be avoided or impaired.

First, in a method of the invention, an implant member is provided. The implant member may be a fillable, elastomeric implant shell having a configuration of a breast prosthesis. Such shells are intended to be filled, typically, with saline or silicone gel before or after implantation in the breast.

Generally, manufacture of such shells is commonly accomplished by applying a liquid dispersion, for example, a silicone elastomer dispersion, to a mandrel having a desired form. The dispersion generally contains a silicone elastomer and a solvent. The silicone elastomer may be polydimethylsiloxane, polydiphenyl-siloxane or some combination of these two materials. Typical solvents include xylene, trichloromethane, heptane, hexane, and toluene.

The silicone dispersion forms an elastomeric coating on the mandrel. The coating is cured and the solvent evaporates therefrom. This procedure may be repeated a

number of times in order to obtain an implant shell having a desired thickness. This shell may be used as base component for many of the implants of the present invention.

In accordance with one aspect of the invention, an implantable member having a desired surface topography is provided. The method comprises the steps of applying a curable fluid composition to a substrate, for example, a surface of an implant shell described above, applying a particulate material to the composition, and in some instances, repeating these steps to achieve layers, for example, alternating layers of composition and particulates. The composition includes a leachable component to be described elsewhere herein. The composition layers are allowed to stabilize between subsequent applications.

Once the layering steps are completed, the composition is subject to conditions to allow it to at least partially cure. Curing process steps will depend on the materials

20 used. One or more process steps are performed to remove the particles of the particle layer(s) and the leachable component from the elastomer.

The resulting implant has an external surface at least a portion of which is an open-cell porous structure having a topography or porosity that affects capsule formation and/or adhesion of the implant when implanted in a patient.

The curable fluid composition may be in the form of an emulsion, dispersion, solution, suspension or mixture containing an elastomer component, a solvent component and a leachable component.

The elastomer component may be an uncured silicone solver, for example, a silicone elastomer. For example, in

some embodiments, the elastomer component is a room temperature vulcanizing (RTV) silicone elastomer. The elastomer component may be polydimethyl siloxane, polydiphenyl siloxane or a combination of these two.

- 5 Possible silicone elastomer systems useful in the present invention include, but are not limited to, oxime, platinum or tin catalyst based systems. Alternatively, the elastomer component may be a non-silicone based material.
- The solvent component may be any suitable solvent or solvent system, appropriate to the elastomer.

Representative examples of solvents include chloroform, acetone, water (buffered saline), dimethyl sulfoxide (DMSO), propylene glycol methyl ether (PM), isopropyl alcohol (IPA),

- n-propyl alcohol, methanol, ethanol, tetrahydrofuran (THF), dimethylformamide (DMF), dimethyl acetamide (DMAC), N-Methylpyrrolidone (NMP), benzene, toluene, xylene, hexane, cyclohexane, heptane, octane, pentane, nonane, decane, decalin, ethyl acetate, butyl acetate, isobutyl acetate,
- isopropyl acetate, butanol, diacetone alcohol, benzyl alcohol, 2-butanone, cyclohexanone, dioxane, methylene chloride, carbon tetrachloride, tetrachloroethylene, tetrachloro ethane, chlorobenzene, 1,1,1-trichloroethane, formamide, hexafluoroisopropanol, 1,1,1-trifluoroethanol,
- and hexamethyl phosphoramide and combinations thereof. In one embodiment, the solvent is selected from the group of solvents consisting of xylene, pentane, hexane, heptane, dichloromethane, trichloromethane, toluene, dimethyl sulfoxide, dioxane, NMP, DMAC, and combinations thereof.
- 30 The solvent component may comprise one or more different solvents. For example, the solvent component may comprise between one and twenty different solvents. Generally, the solvent may comprise any suitable protic or aprotic solvent, mixture or solution thereof.

The leachable component is a leachable material/agent in the form of any suitable solid particulates, semi-solids, composites, gels, for example, hydrogels, liquid droplets, etc. The leachable agent may comprise any suitable polymer, ceramic, metal, composite or combination thereof that can be dissolved or otherwise removed by suitable means from the cured formulation. In some embodiments, the composition comprises one or more different leachable agents. For example, the composition may comprise between one and twenty different types of leachable agents.

The elastomer component can be present in the composition in a range of about 1% to about 99% of volume as part of the total dissolved solids and the leachable agent

15 can be in the range of about 1% to about 99% of volume as part of the total dissolved solids. In a specific embodiment of the invention, the composition includes up to 96% leachable phase. In some embodiments, the elastomer component is present in the composition in a range of about 5% to about 80% and the leachable agent is present in the composition in a range of about 20% to about 95% of total dissolved solids. Generally, the total dissolved solids in the composition can range from about 1% to about 50% by weight in solution.

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The ratio of leachable phase to matrix phase in the composition generally affects the porosity of the final cured composition. For example, a greater percentage of leachable component in the composition will produce a composition layer having greater interconnections between pores.

In an exemplary embodiment, the curable fluid composition is in the form of an emulsion, and the leachable agent is present in a concentration of up to about 50%

concentration by volume of the emulsion. In some embodiments, the composition comprises a microphase separation containing an elastomer matrix phase and droplets of leachable material in suspended phase, the droplets being about 0.01 µm to about 10,000 µm in diameter, for example, about 1 µm to about 5,000 µm in diameter, for example, about 50 µm to about 400 µm in diameter. After the leachable agent has been leached from the elastomer, voids left behind by the leachable agent will serve as interconnections between voids left by the removed particles.

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The leachable agent may be, for example, any material that can be dispersed through the elastomer dispersion (elastomer component/solvent system) and can be removed therefrom once the elastomer component is cured. The leachable agent may be an agent that can be removed from the cured elastomer, for example, by leaching, evaporation, sublimation, dissolution, etc. In an exemplary embodiment, the leachable agent is a water soluble material dispersed throughout the elastomer dispersion.

Typical leachable agent in accordance with the invention may comprise, for example, polyethylene glycol (PEG) (also known as polyoxyethylene), polyalkylene oxides including polyethylene oxide and polyethylene oxide/polypropylene oxide copolymers (also known as poloxamers), polyhydroxyethylmethacrylate, polyvinylpyrrolidone, polyacrylamide and its copolymers, polylactides, polyglycolides, polyanhydrides, polyorthoesters and their copolymers, proteins including albumin, peptides, liposomes, cationic lipids, ionic or nonionic detergents, salts including potassium chloride, sodium chloride and calcium chloride; sugars including galactose, glucose and sucrose; polysaccharides including

soluble celluloses, heparin, cyclodextrins and dextran; and any combination thereof.

In some embodiments, the leachable agent is an agent selected from the group of agents consisting of polyvinlyl alcohol, polyethylene glycol, polyacrylic acid, polymethacrylate, poly-lactide, polyglycolide, polycaprolatone, polydioxanone; and derivatives, blends, copolymers, terpolymers, and combinations thereof.

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In some embodiments, the leachable agent is in the form of droplets of leachable material having diameters in a range of between about 0.01 micron to about 10,000 microns. For example, the leachable agent may be in the form of droplets having diameters in a range of between about 1 micron to about 5,000 microns, for example, in a range of between about 50 microns to about 400 microns.

The particulates of the particle layer comprise any suitable particles which may be removed from the cured elastomer, leaving cavities where the particles had been.

For example, the particles may comprise particles that can be removed from the elastomer by at least one of mechanical abrasion, leaching, evaporation, sublimation, dissolution etc.

In an exemplary embodiment, the particles are a solid, water soluble material. For example, the particles may be material selected from the group of materials consisting of sodium chloride, barium sulfate, potassium nitrate and sodium carbonate.

In addition, the particles may have dimensions and shapes as desired to bring about a resulting topography. For

example, the particles may be substantially round or spherical, mutifaceted, angular, or cubic or a combination thereof. The particles may have an average particle size in a range of between about 0.01 micron to about 10,000 microns, for example, in a range of between about 10 microns to about 6,000 microns, for example, in a range of between about 100 microns to about 900 microns.

In some embodiments, the size of the particles is

approximately proportional to the thickness of the
composition coating on which they are deposited, or the
thickness of adjacent interconnecting composition coatings
in a multilayered embodiment. For example, particles with
an average size of about 500 micron could be used in

conjunction with a composition layer having a thickness of
about 100 microns to about 500 microns. For particles with
an average size of about 300 microns, a composition layer of
about 50 microns to about 400 microns could be used.

Figures 1A-1C illustrate an exemplary process for making an implant in accordance with an embodiment of the invention. Step one is illustrated in 1A. In Fig. 1A, a flexible, elastomeric implantable member 12 is depicted. The partial cross sectional view 11 of the elastomeric implant member 12 is shown in Fig. 1A as well as Fig. 2. The implantable member 12 may be a cured implant shell, such as a conventional, relatively smooth-surfaced, silicone-based elastomeric implant shell, for example, a shell intended to be filled with silicone gel or saline and used as a breast prosthesis.

A curable fluid composition 14, as described elsewhere herein, is applied to the outer surface of the shell 12. Figure 3 shows a partial cross sectional view of a shell 12 having a composition coating 10. This may be accomplished

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by dipping the shell (as shown by shaded line 13), while the shell is fixed to a mandrel (not shown) into a solution bath containing the curable fluid composition 14 (Fig. 1A). The composition 14 comprises a silicone-based mixture including a solvent, and a leachable agent, as described elsewhere herein. The step of applying the composition 14 to the shell 12 may be accomplished by any suitable means of application, such as dipping and spraying.

10 Next, the composition coating is allowed to stabilize on the shell 12. For example, the shell 12 can be held in a stable position until the composition coating no longer flows freely. This occurs as some of the solvent evaporates from the coating, raising its viscosity. It can be 15 appreciated that the step of allowing the composition to stabilize may be accomplished by various means, for example, by allowing some of the solvent to evaporate out of the composition or allowing a chemical reaction to occur, inducing precipitation of the soluble components. 20 Alternatively, stabilization can be achieved during crosslinking of polymerization of the silicone, or precipitation of the silicone or pore-forming material.

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Once the composition 14 has stabilized on the shell
12, the second step is to immerse (see shaded line 15) the
shell 12 in a particle bath 16 to apply particles to the
composition coating on the shell 12 (Fig. 1B). The

30 particles 18 applied to a composition-coated shell 12 is
depicted in Fig. 1B. Fig. 4 shows a partial cross sectional
view of a shell 12 with a composition coat 10 and particles
18. Application of the particle coating onto the shell 12,
is performed while the composition coating on the shell 12
35 is still tacky and able to retain the particles. Stabilizing

Also, a combination of the above-mentioned methods may be

used for stabilization of the composition coating.

the composition prior to particle application may be accomplished by allowing at least some of the solvent in the composition to evaporate out of the composition until the composition is stable and tacky but not fully cured.

5 Another method, in accordance with one aspect of the invention, for stabilizing the composition is provided in the Example below.

Steps one and two can be repeated before the leaching step is carried out, as indicated by shaded line 17. The steps of applying a curable fluid composition and applying a particle coating can be repeated, for example, one or more times, for example, three, five or even up to 20 times, until a final coating is applied. The final coating may be a particle or a composition coating.

After the final coating of particles or fluid composition is applied to the shell, the coated shell is then subjected to suitable curing conditions to solidify the composition with the particles embedded therein.

20 after the solidification step described above, the embedded particles and leachable agent in the composition coating are immersed in a leaching bath 20 and removed. After the removal of the particles, what remains is a network of interconnected pores 21(the structure may include both relatively large pores and relatively smaller pores, for example, micropores) on the shell.

Also see Fig. 7 for a flow chart of the process described herein.

30 EXAMPLE 1

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A mixture of about 7.5 wt. % PVA 2000 in water and about 40 wt. % acetoxy RTV silicone in xylene in a 3:1 volumetric ratio is prepared and homogenized for 30 seconds.

35 An acetyl mandrel is placed into the mixture and coated

uniformly as in a standard dip-coating process for the manufacturing of breast implant shells. The mandrel is then placed into a fluidized bed reactor with salt granules until no more granules can be deposited on the mandrel (about 5-10 seconds). This addition of salt particles tends to dry and stabilize the mixture by absorbing some of the water, thereby increasing the viscosity of the mixture. The coating is allowed to stabilize further at either 90°C for about 15 minutes or at room temperature for about ½ hour, or otherwise sufficiently such that the next layer of composition may be applied. The procedure is repeated 3-5 times to obtain a coating of desired thickness.

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Final curing may be performed at 165°C for 2 hours,

15 leaching with water or DCM for about 30 minutes for about 3

cycles with each (with agitation), and drying in vacuum overnight.

In one embodiment, a material is added to the

composition before or after the composition has been applied to the shell, the material being effective to increase the viscosity of the composition, for example, by absorbing some of the solvent. When the leachable agent is in water, for example, a salt can be added in order to dry/stabilize the

phase by absorbing the solvent. Other materials that may be helpful in this regard include sugars and other appropriate materials that can accelerate removal of solvent from the composition.

Next, a particle coating is applied to the composition to form the pores or cavities in the final elastomer foam structure. Application of the particles may be accomplished by any suitable means, for example, by sprinkling and pressing the particles into the tacky composition coating, or by immersing the tacky, coated shell in a bath of the

particles. In the example shown, the particles are applied by immersing the coated shell into a fluidized bath 18 comprising a fluidization medium 19, for example, air, and particulates, for example, salt particles.

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In some embodiments, the steps of applying the curable fluid composition and applying the particle coating are then repeated one or more times, for example, from about 0.5 up to about 20 times, for example, about 1 to about 10 times, for example, about 2 to about 5 times.

In one aspect of the invention, the particle coatings applied to the composition coatings may comprise coatings of particles having relatively different dimensions, one layer from the other. In other words, a first layer of particles may be relatively fine particles and a second layer of particles may be relatively coarse particles, or vice versa.

It is contemplated that in some embodiments,

interconnectivity between pores may be increased or

controlled by causing the particulates in the particle layer

to fuse together. For example, in the event that the

particles are salt crystals, application of moist heat may

be effective increase interconnectivity thereof.

- 25 Alternatively or additionally, an appropriate amount of a solvent for the particle material may be applied in order to cause the particles to fuse together. Further information which may be useful in appreciating this aspect of the invention may be found in copending, commonly owned U.S.
- 30 Provisional Patent Application No. 61/177,955, filed on May 13, 2009 and entitled: IMPLANTS AND METHODS FOR MANUFACTURING SAME, the entire disclosure of which is incorporated herein by this reference.

For example, in one embodiment, the steps of applying alternating particle and compositions coatings includes applying a first layer of the curable fluid composition to the shell, applying a first layer of particles, for example, 5 relatively small particles, to the composition, applying a second layer of the composition to the first layer of particles, applying a second layer of particles, for example, relatively larger particles, to the second layer of the composition. Fig. 5 is a cross sectional view of a 10 shell showing alternating layers of compositions coatings 10 and particle coatings 18. In a specific embodiment, the first layer of particles comprises particles having an average size in a range of between about 30 microns to about 150 microns, and the second layer of particles comprises 15 particles having an average size in a range of between about 100 microns to about 450 microns. In yet other embodiments, the method further includes applying a third layer of the composition to the second layer of particles, and optionally, providing a third layer of particles, to the 20 third layer of composition. The third layer of particles may have an average size in a range of between about 250 microns to about 750 microns.

The layered, coated shell is then subjected to suitable curing conditions to solidify and further stabilize the composition with the particles embedded therein.

Next, the particles and leachable agent are then removed from the cured coating, thereby revealing a network of highly interconnected pores within the cured elastomer. Fig. 6 shows the partial cross sectional view of the shell 11 with a network of interconnected pores 21 after the removal of the particles. The step of removing the particles may comprise causing the particles to dissolve or contacting the particles with an abrasive surface. In the

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same step or in a different step, the leachable agent in the composition layers are removed from the elastomer.

In some embodiments, a conventional gas foaming process is used in addition to one or more of the presently described processes of the invention. For example, prior to the steps of applying the composition to the shell, the composition may be aerated by passing a gas, for example, air, through the composition to aerate the composition and create bubbles therein. Advantageously, any surface skin that may begin to form on the aerated composition coating would be opened up during extraction of the leachable phase to reveal highly interconnected pores resulting from the leachable materials, the particulates and the gas bubbles.

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Removal of the particles and leachable agents may be accomplished by extracting these materials by exposing the layers to one or more suitable mediums capable of dissolving the particles and/or leachable agents. For example, the coated shell is dipped or submerged in a leaching bath 19 (Fig. 1C). The leaching bath may comprise water or an aqueous solution containing an agent capable of dissolving, leaching or otherwise removing the leachable agent and/or particles while leaving the cured elastomer substantially intact.

In some embodiments, the particles which are typically larger than the dispersed leachable agent, serve to create pores in the cured elastomer and the dispersed leachable agent serves to create micropores or interconnections between the relatively larger pores.

The resulting open-cell structure is believed to facilitate tissue ingrowth, improve fixation or adhesion of the implant and discourages organization of the collagen

capsule which forms about the implant, which may help reduce capsular contraction.

In another aspect of the invention, an implantable

5 composite member is provided in which the composite member has an external surface at least a portion of which is an open-cell porous structure, the composite member being made by one of the processes described herein.

In yet other embodiments of the invention, each of the first and second layers of particles are made up of substantially uniformly sized/shaped particles. In another aspect of the invention, each of the first and second layers of particles are made up of differently sized or shaped components.

After finishing the shell according to the steps described above, the steps required to make a finished mammary prosthesis may be conventional. First, any opening left by the mandrel support is patched with uncured silicone elastomer sheeting. If the prosthesis is to be filled with silicone gel, this gel is added and cured, the filled prosthesis packaged, and the packaged prosthesis sterilized. If the prosthesis is to be inflated with a saline solution, a valve is assembled and installed, the prosthesis is post cured if required, and the prosthesis is then cleaned, packaged and sterilized. A combination silicone/saline mammary prosthesis can also be made.

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A method has been described for creating an outer layer having an open-cell structure in a silicone elastomer member. More specifically, the method can be applied to create a medical implant with an external surface layer of silicone elastomer having an open-cell structure, to create strips having a textured surface for control of scar

formation, or to improve a process for making mammary prostheses. The product made by this method has also been described and is expected to have great utility in reducing capsular contraction, in preventing or controlling scar formation, and in anchoring medical implants.

Scar tissue formation in the healing of a wound or surgical incision is also a process involving the growth of fibrous tissue. A visible scar results from this healing process because the fibrous tissue is aligned in one direction. However, it is often aesthetically desirable to prevent scar formation, especially in certain types of plastic surgery. A member having an open-cell structure surface made in accordance with the present invention can be placed subcutaneously within a healing wound or incision to prevent the fibrous tissue from aligning and thereby prevent or reduce scar formation.

against movement. Mammary prostheses are one example of implants that must be anchored. Facial implants are another example of implants that must be anchored. With facial implants it is particularly important that they be anchored securely against movement because of their prominent

25 location. Providing such implants with an open-cell structure surface made in accordance with the present invention is a particularly advantageous way to ensure that they will be anchored securely.

30 EXAMPLE 2

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A composition is prepared by mixing polyethylene glycol monomethyl ether (2000 Da), which will serve as a leachable agent, with a low viscosity silicone elastomer dispersion, for example, (e.g. polydimethylsiloxane,

polydiphenylsiloxane, poly(dimethylsiloxane-co-diphenylsiloxane), poly(dimethylsiloxane-ran-diphenylsiloxane), etc.), in an organic solvent (e.g. xylene), and at about 5 to about 40 wt%, or in some specific embodiments, 17, 25 and 35 wt% of acetoxy RTV silicone.

This composition is applied to the surface of an elastomeric shell held on a mandrel or other mechanical support. The layer is allowed to evaporate most of the solvent off.

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A coating of sodium chloride crystals (about 250 μm to about 850 μm size) are applied to the tacky composition layer by submerging the coated shell into a fluidized bath of salt and air. This forms a relatively uniformly distributed single layer particle coating.

The elastomer is allowed to evaporate the solvent off and subsequently cured at approximately $145\,^{\circ}\text{C.}$

20 The coated shell is then submerged in an aqueous washing medium at approximately 40°C and gently agitated to remove the particles and leachable agent.

EXAMPLE 3

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The same process is performed as in Example, 1, except that the composition is a mixture of 10mL xylene, 10mL DCM, 5mL by dry volume PEG 2000 and 5mL by dry volume acetoxy RTV silicone elastomer.

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EXAMPLE 4

The same process is performed as in Example 2, except that the composition is a mixture of

35 5mL water

1mL xylene

0.5mL by dry volume PVA 1500

0.2mL by dry volume RTV.

In another aspect of the invention, an article, for 5 example a thin, flexible sheet, useful as a laminate, is provided. More specifically, the present invention provides a biocompatible sheet suitable for use as a laminate on an implantable device or object, in order to enhance tissue 10 adhesion or ingrowth when the implantable device or object is implanted in a patient. Thus, the manufacture of the materials in accordance with the invention is not limited to conventional dipping processes but may be made by other suitable means, for example, through the lamination of a 15 sheet that is prepared by molding or casting. For example, it is contemplated by the inventors that a sheet or laminate can be prepared by casting the fluid material with all the components present in various ratios (DCM, PEG) + (Xylene, RTV), and in some instances, mixed and shaken with the 20 particulate component, for example, salt crystals added to the liquid. The particulate and fluid mixture can be shaken or mixed and cast onto a substrate or into a mold cavity. In some embodiments, the particulate component comprises salt in a range of about 10% to about 99% of total dissolved 25 solids. In a more specific embodiment, the salt is present at about 25% to about 60%. It can be appreciated that different amounts and different particle sizes/shapes of salt will produce laminates having different porosities. Once cured, the laminate can be laminated, by any conventional means known in the art, onto a medical device 30 or implant or other object to be implanted in a body, for example, any object or device which would be improved by the addition of such a laminate on one or more surfaces of the object or device. For example, the sheet may be laminated

to catheter cuffs for long term implantable catheters, duramatter substitutes or the like.

EXAMPLE 5

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A laminate for an implant is prepared as follows. A fluid composition made up of 10mL xylene, 10mL DCM, 5mL by dry volume PEG 2000 and 5mL by dry volume acetoxy RTV silicone elastomer is mixed with 3.5 mL by volume salt particles. This mixture is shaken together to ensure substantially uniform distribution of particles. mixture is cast molded by applying the mixture to a mold surface to form a layer having a uniform thickness of between about 1 mm to about 5 mm. The layer is allowed stabilize and is cured at about 120° C for a sufficient period of time. The cured sheet is removed from the mold surface and is then contacted with a gentle spray of pure water to remove all of the leachable components and salt particles. The resulting, thin, flexible, porous silicone foam sheet is then further processed and sterilized and packaged for sale or storage for later use as a laminate on a surface of an implantable device.

EXAMPLE 6

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The process of Example 5 is performed with the additional steps of repeating, three times, the step of applying a fluid composition/particulate mixture to the stabilized layer prior to the step of curing. The final thin, flexible sheet is a multilayered sheet and, in this example, has a thickness of greater than about 5 mm.

EXAMPLE 7

The process of Example 5 is performed, however the cured stabilized sheet is not contacted with a spray of water to remove the leachable agents and particulates before being packaged for sale or storage. Instructions are provided with regard to: removing the leachable agents and particulates, sterilization, and bonding the sheet to a surface of a medical device.

10 EXAMPLE 8

The process of Example 5 is performed to make two square sheets of uncured foam, approximately 240mm X 240mm. A layer of silicone adhesive in DCM is applied, by spraying or brushing, to one side of each of the sheets. The sheets are stretched uniformly and positioned one on top of the other, adhesive side facing each other, over a newly molded breast implant shell filled with silicone or air. The foam sheets are joined together at the edge of the implant and affixed by suitable clamps at the perimeter of the implant. Twenty four hours later, the clamps are removed. Excess foam is die-cut away from the implant by a press. The implant/foam is exposed to 140°C for 2.5 hours for final post-curing.

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While this invention has been described with respect to various specific examples and embodiments, it is to be understood that the invention is not limited thereto and that it can be variously practiced within the scope of the invention.

What is claimed is:

1. An implantable member having an external surface at least a portion of which is an open-cell porous structure, the member made by the method comprising the steps of:

- (a) providing an implantable shell;
- (b) applying a curable fluid composition to the shell, the composition comprising a mixture containing an elastomer component, a leachable agent and a solvent component;
- (c) applying a layer of particles to the composition;
- (d) allowing the composition to stabilize; and
- (e) removing the particles and the leachable agent from the stabilized composition to form a composite material having an external surface at least a portion of which is an opencell porous structure.
- 2. The member of claim 1 wherein the implantable shell is a shell for a breast implant.
- 3. The member of claim 1 wherein the leachable agent is a water soluble polymer.
- 4. The member of claim 1 wherein the leachable agent is an agent selected from the group of agents consisting of polyvinyl alcohol, polyethylene glycol, polyacrylic acid; polymethacrylate, poly-lactide, polyglycolide, polycaprolatone, polydioxanone, derivatives thereof, blends thereof, copolymers thereof, terpolymers thereof, and combinations thereof.
- 5. The member of claim 1 wherein the solvent component includes a solvent selected from the group consisting of xylene, pentane, hexane, dichloromethane (DCM), dimethyl sulfoxide, dioxane, NMP, DMAc, and combinations thereof.

6. The member of claim 1 wherein the mixture is an emulsion.

- 7. The member of claim 1 wherein the particles comprise a material selected from the group of materials consisting of sodium chloride, barium sulfate, potassium nitrate, sodium carbonate.
- 8. The member of claim 1 wherein the particles are substantially round.
- 9. The member of claim 1 wherein the leachable agent is in the form of droplets having diameters in a range of between about 50 microns to about 400 microns.
- 10. The member of claim 9 wherein the particles have an average particle size in a range of between about 100 microns to about 900 microns.
- 11. The member of claim 1 wherein the particles have an average particle size in a range of between about 100 microns to about 900 microns.
- 12. The member of claim 1 further comprising the step of repeating steps (b) and (c) prior to the step of removing, to form a layered structure.
- 13. The member of claim 1 wherein the step of removing comprises contacting the stabilized composition with a solvent for the particles and the leachable agent.
- 14. An implantable composite member having an external surface at least a portion of which is an open-cell porous structure, the member made by the method comprising the steps of:

- (a) providing an implantable shell;
- (b) applying a first layer of a curable fluid composition to the shell, the composition comprising a mixture containing an elastomer component, a leachable agent and a solvent component;
- (c) applying a first layer of particles to the composition;
- (d) applying a second layer of the composition to the first layer of particles;
- (e) applying a second layer of particles to the second layer of the composition;
- (f) allowing the composition to stabilize; and
- (g) removing the particles and the leachable agent from the stabilized composition to form a composite material having an external surface at least a portion of which is an opencell porous structure.
- 15. The member of claim 14 wherein the first layer of particles comprises relatively small particles and the second layer of particles comprises relatively large particles.
- 16. An article suitable for use in as a laminate for an implant, the article comprising:
- a flexible sheet made by the process of:
- (a) applying a particulate component and a curable fluid composition to a mold surface, the fluid composition comprising a mixture containing an elastomer component, a leachable agent and a solvent component;
- (b) allowing the fluid composition component to stabilize; and
- (c) removing at least one of the particulate component and the leachable agent from the stabilized composition to form a sheet having an external surface at least a portion of which is an open-cell porous structure; and
- (d) removing the sheet from the mold surface.

17. An article comprising:

a sheet suitable for use as a laminate on an implantable object to enhance tissue adhesion or ingrowth when the implantable object is implanted in a patient;

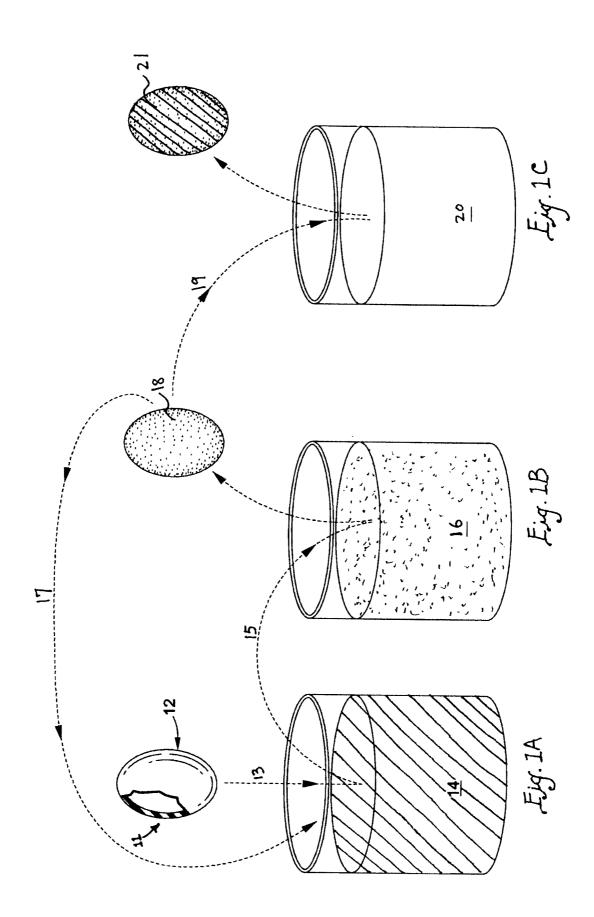
the sheet made by a process comprising the steps of:

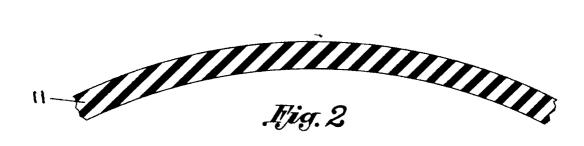
applying a fluid/particulate mixture to a substrate or mold surface, the fluid/particulate mixture comprising a particulate component and a curable fluid component, the curable fluid component containing an elastomer component, a leachable agent and a solvent component;

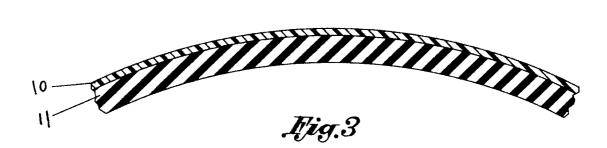
allowing the fluid/particulate mixture to stabilize; and

removing the sheet from the substrate or mold surface.

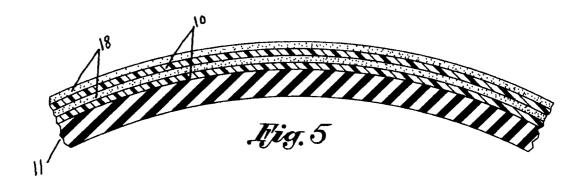
- 18. The article of claim 17 further comprising the step of removing at least one of the particulate component and the leachable agent from the stabilized fluid/particulate mixture to form a porous sheet after the step of allowing the fluid/particulate mixture to stabilize.
- 19. The article of claim 18 wherein the step of removing at least one of the particulate component and leachable agent is performed prior to the step of removing the sheet from the substrate of mold surface.
- 20. The article of claim 17 wherein the sheet is a layered sheet and the process further comprises the step of repeating the applying step prior to the step of removing the sheet from the substrate or mold surface.



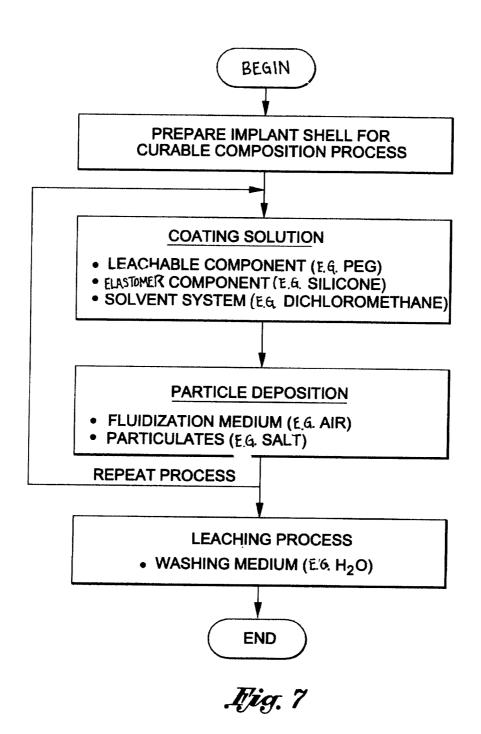












INTERNATIONAL SEARCH REPORT

International application No PCT/US2010/051838

A. CLASSIFICATION OF SUBJECT MATTER INV. A61L27/30 A61L27/56 ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61L

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, BIOSIS, EMBASE, INSPEC, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT					
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.			
X	WO 2009/061672 A1 (ALLERGAN INC [US]; POWELL THOMAS E [US]; DANG LOANTRANG [US]) 14 May 2009 (2009-05-14) page 2, line 17 - line 23 page 3, line 5 - line 17 page 8, line 11 - line 17 page 10, line 8 - line 30				
X	US 4 889 744 A (QUAID JOEL [US]) 26 December 1989 (1989-12-26) column 3, line 37 - line 58 column 4, line 3 - line 21 column 5, line 12 - line 68 column 6, line 4 - line 6 column 7, line 1	1,2,5,7, 8,11-20			

Further documents are listed in the continuation of Box C.	X See patent family annex.				
"A" document defining the general state of the art which is not considered to be of particular relevance "E" earlier document but published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed	 "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. "&" document member of the same patent family 				
Date of the actual completion of the international search 18 February 2011	Date of mailing of the international search report $01/03/2011$				
Name and mailing address of the ISA/ European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Fax: (+31-70) 340-3016	Authorized officer Laurent, Antoine				

INTERNATIONAL SEARCH REPORT

International application No
PCT/US2010/051838

ategory*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
ategory*	Citation of document, with indication, where appropriate, of the relevant passages US 5 545 220 A (ANDREWS WINSTON A [US] ET AL) 13 August 1996 (1996-08-13) column 2, line 12 - line 23 column 3, line 1 - line 45	Relevant to claim No. 1,2,8, 11-20

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No
PCT/US2010/051838

Patent document cited in search report		Publication date	Patent family member(s)			Publication date
WO 2009061672	A1	14-05-2009	CA EP US	2704697 A1 2227175 A1 2009118829 A1	•	14-05-2009 15-09-2010 07-05-2009
US 4889744	Α	26-12-1989	AU AU	617667 B2 1522388 A	 -	05-12-1991 02-11-1989
US 5545220	A	13-08-1996	AT AU AU BR CA DE DE EP WO	224741 T 683733 B2 1895195 A 9407978 A 2175898 A1 69431438 D1 69431438 T2 0726782 A1 9512419 A2	- - - -	15-10-2002 20-11-1997 23-05-1995 03-12-1996 11-05-1995 31-10-2002 27-11-2003 21-08-1996 11-05-1995